The bone ecosystem facilitates multiple myeloma relapse and the evolution of heterogeneous proteasome inhibitor resistant disease.

Authors/affiliations

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Abstract

Multiple myeloma (MM) is an osteolytic plasma cell malignancy that, despite being responsive to therapies such as proteasome inhibitors, frequently relapses. Understanding the mechanism and the niches where resistant disease evolves remains of major clinical importance. Cancer cell intrinsic mechanisms and bone ecosystem factors are known contributors to the evolution of resistant MM but the exact contribution of each is difficult to define with current *in vitro* and *in vivo* models. However, mathematical modeling can help address this gap in knowledge. Here, we describe a novel biology-driven hybrid agent-based model that incorporates key cellular species of the bone ecosystem that control normal bone remodeling and, in MM, yields a protective environment under therapy. Critically, the spatiotemporal nature of the model captures two key features: normal bone homeostasis and how MM interacts with the bone ecosystem to induce bone destruction. We next used the model to examine how the bone ecosystem contributes to the evolutionary dynamics of resistant MM under control and proteasome inhibitor treatment. Our data demonstrates that resistant disease cannot develop without MM intrinsic mechanisms. However, protection from the bone microenvironment dramatically increases the likelihood of developing intrinsic resistance and subsequent relapse. The spatial nature of the model also reveals how the bone ecosystem provides a protective niche for drug sensitive MM cells under treatment, consequently leading to the emergence of a heterogenous and drug resistant disease. In conclusion, our data demonstrates a significant role for the bone ecosystem in MM survival and resistance, and suggests that early intervention with bone ecosystem targeting therapies may prevent the emergence of heterogeneous drug resistant MM.

Introduction

Multiple myeloma (MM) is the second most common hematological malignancy in the US[1], characterized by the clonal expansion of plasma cells localized primarily in the bone marrow microenvironment of the skeleton [2,3]. In the bone microenvironment, MM cells disrupt the finely tuned balance of trabecular and cortical bone remodeling to generate osteolytic lesions. This is primarily via MM-induced inhibition of osteoblastic bone formation and increase of osteoclastic bone resorption. There are currently several approved therapies to treat MM including, but not limited to, proteasome inhibitors (e.g., bortezomib and carfilzomib), chemotherapy (e.g., melphalan), immunomodulatory drugs (e.g., lenalidomide), and cellular and non-cellular immunotherapies (e.g., B cell maturation antigen (BCMA) chimeric antigen receptor- (CAR) T cells and daratumumab) that significantly contribute to the long-term survival of MM patients[4]. However, MM remains fatal as nearly all patients ultimately become refractory to various lines of therapy. A greater understanding of how resistant MM emerges in the clinical setting can yield new treatment strategies to slow relapse times and extend the efficacy of standard of care therapies.

In MM and other cancers, the tumor microenvironment is a well-known contributor to the development of treatment resistance[5-10]. MM is an archetype of cancer cell-stroma interactions whereby MM cells reside and metastasize systemically within the bone marrow microenvironment[11]. In the bone ecosystem, MM interacts closely with mesenchymal stem cells (MSCs) and other progenitor cells[6,12-15] that secrete MM pro-survival and proliferative factors. Additional studies have shown that the bone marrow microenvironment can also protect MM cells from applied therapy in a phenomenon known as environment mediated drug resistance (EMDR)[7,8,16]. Reciprocally, it is well established that MM-derived factors stimulate osteoblast lineage cells to recruit and activate osteoclasts through receptor activator of nuclear factor kappa-B ligand (RANKL) production, which in turn degrade the bone matrix to release stored cytokines and growth factors (e.g., transforming growth factor-beta, TGF-β) that support MM survival and growth[2,3,5-10]. MM cells also suppress osteoblast maturation, thus tipping the balance towards excessive bone destruction[2,3]. This vicious cycle leads to complications for MM

patients such as hypercalcemia and pathological fracture that greatly contribute to
morbidity and mortality[17].

While EMDR can contribute to drug resistance, MM intrinsic mechanisms, such as
genetic and epigenetic alterations, also play a significant role in the process.   For
example, increased expression of the anti-apoptotic BCL2 protein family is important in
mediating MM resistance to proteasome inhibition[18-21]. In fact, depending on selective
pressures by different lines of therapies and clonal mutation capacity, MM may evolve to
develop multiple mechanisms of resistance[5,22,23]. While EMDR and intrinsic drug
resistance mechanisms contribute to the emergence of refractory disease several
questions remain: i) How does the interplay between each mechanism contribute to the
evolution of resistant MM? ii) How does each mechanism contribute to the heterogeneity
of the disease under either control or treatment conditions? iii) Could targeting EMDR
alter the course of the disease or its responsiveness to applied therapy thereby yielding
significantly greater depths of treatment response? In the context of the bone marrow
microenvironment and the direct/indirect communications occurring in a temporal and
spatial fashion between MM and stromal cells, these questions remain difficult to address
using current *in vivo* and *ex vivo* approaches.

Mathematical models of the tumor microenvironment have become a valuable
approach that allows us to interrogate the interactions between multiple cellular
populations over time under normal or disease conditions. In particular, hybrid cellular
automata (HCA) models which couple discrete cell-based models with partial differential
equations include spatial aspects enabling users to locate where phenomena are
occurring. Further, mathematical models have the potential for clinical translatability and
can be used to study the impact of treatment on the tumor microenvironment and delay
the onset of resistant disease[24-31]. We therefore leveraged these modeling approaches
to examine MM progression and spatial evolution in response to therapy. To this end, we
generated a novel HCA model powered by biological parameters from a mouse model of
MM and demonstrate how it captures both normal bone turnover, and spatiotemporal
cellular dynamics during MM progression in bone, such as loss of osteoblasts, increased
stromal cell infiltration, osteoclast formation, and osteolysis. Additionally, we incorporate
the proliferative and protective bone marrow microenvironment effects on MM mediated

by osteoclastic bone resorption and bone marrow stromal cells. In the treatment setting,

the HCA demonstrates that EMDR contributes to minimal residual disease, protecting

tumors from complete eradication. Moreover, this reservoir of MM cells increases the

likelihood of unique resistance mechanisms arising over time and greatly contributes to

the evolution of MM heterogeneity over time compared to non-EMDR scenarios. These

results highlight the importance of the bone marrow microenvironment in contributing to

MM resistance and patient relapse and provide a strong rationale for targeting both the

MM and bone marrow microenvironment mechanisms for optimal treatment response.

Results

The HCA model recapitulates the key steps of trabecular bone remodeling.

Trabecular bone remodeling is a continuously occurring process that is essential for

regulating calcium homeostasis and bone injury repair (Fig. 1a) [32,33]. This process occurs

asynchronously throughout the skeleton at individual sites known as basic multicellular

units (BMUs). The BMU in our HCA consists of five different cell types, including precursor

osteoclasts, active osteoclasts, mesenchymal stem cells (MSCs), preosteoblasts, and

osteoblasts. Additionally, we include central signaling molecules such as RANKL, a driver

of preosteoclast motility and OC formation[34] and osteoclastic release of bone derived

factors (BDFs) such as transforming growth factor beta of which bone is a major

reservoir[35]. In the HCA, we use TGF-β as a representative BDF given its known biphasic

effects on cell behavior and its concentration dependent ability to modulate preosteoblast

proliferation and maturation to bone forming osteoblasts[36-40]. We defined the roles and

interactions of these key cellular populations and the factors that govern their behavior

during the remodeling process using parameters derived experimentally or from the

literature (Fig. 1b-c, Supp Fig. 1a and Supplementary Tables 1-6). It is important to note

that each cell in the HCA behaves as an autonomous agent that can respond to

surrounding environmental cues independently. In our HCA model, new bone remodeling

events are initiated over time at randomly selected locations such that multiple BMUs may

be present at a given time as opposed to our previous HCA model[27,41-43]. We

demonstrated that each BMU undergoes five key phases of bone remodeling: initiation,

resorption, reversal, formation, and quiescence[44] ultimately returning to homeostasis (Fig.

2 and Supplementary Video 1). We also observed that each simulation (n = 25) generated

multiple BMUs over time, resulting in the replacement of the majority of the bone over a

four-year period (Fig. 2, Supplementary Video 1, Supplementary Fig. 1). We also noted

that while the bone area to total area (BA/TA) remains relatively constant the shape of

the trabecular bone changes, underscoring the dynamic nature of HCA model and how it

reflects the *in vivo* scenario.

The HCA model captures dose-dependent effects of BDF and RANKL

To challenge the robustness of our bone remodeling HCA, we altered the levels of key

factors controlling bone homeostasis. Our *in vitro* experimental data show that

neutralizing TGF-β or addition of exogenous TGF-β in osteoblastic cell cultures increases

and decreases mineralization respectively, a finding that is consistent with the

literature[35,40,45] (Supplementary Fig. 2a). Similarly, lowering TGF-β levels *in silico* led to a

dramatic increase in bone volume (Supplementary Fig. 2b-e). Interestingly, the HCA

results showed that when TGF-β levels dropped below 90%, there was significant bone

loss (Supplementary Fig. 2b-e) due to abrogation of MSC proliferation leading to reduced

numbers of preosteoblasts that contribute to bone formation (Supplementary Fig. 2e).

These data are reflective of the known biphasic roles of TGF-β on cell behaviors and

processes at high and low concentrations[35,40,45]. In addition, we demonstrated the

sensitivity of OC formation in the HCA model in response to changes in RANKL levels

(Supplementary Fig. 2f-h). These data demonstrate that the complex HCA model can

integrate the behaviors and responses of multiple highly coupled cell types and stimuli to

achieve responses reflective of known biology.

The HCA model integrates the impact of standard of care therapies on bone

remodeling.

Next, we assessed the response of the HCA model to standard of care therapies used

for the treatment of MM such as zoledronate (ZOL) and bortezomib (BTZ). These

compounds can block osteoclast function and formation respectively but, as we and

others have shown, they can also stimulate osteoblast mediated bone formation[46-49]

(Supplementary Fig. 3a-b and Supplementary Fig. 4a-b). Our results show that, as
expected, both ZOL and BTZ therapy increased bone volume over the treatment period
by enhancing osteoblastic bone formation and blocking osteoclast activity/formation
(Supplementary Fig. 3c-h, Supplementary Fig. 4c-h). While osteoclasts are impacted by
both treatments, the HCA recapitulates their distinct mechanisms of action showing that
ZOL targets actively resorbing osteoclasts as demonstrated by a reduction in bone
resorption per OC (Supplementary Fig. 4h) while BTZ limits the fusion of osteoclast
precursors as shown by a reduction in cumulative osteoclast numbers with treatment
(Supplementary Fig. 3g). Collectively, these data demonstrate the ability of our HCA
model to capture normal bone remodeling over extended periods and the appropriate
response of the model to applied therapeutics used for the treatment of MM.
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The HCA model incorporates the MM-bone ecosystem vicious cycle.
A key component of MM growth involves the initiation of a feed-forward vicious cycle
leading to reduced bone formation and enhanced osteoclastic bone destruction (Fig. 1a).
MM is also known to interact with several cellular components of the bone ecosystem
such as MSCs[2,16]. To incorporate these effects and MM growth characteristics into the
HCA, mice were inoculated with U266-GFP MM cells and at end point, bones were
processed and stained for proliferation (Histone H3 phosphorylation (pHH3)) and
apoptosis markers (Terminal deoxynucleotidyl transferase dUTP nick end labeling
(TUNEL)). Our data show that the highest proportion of proliferating MM cells are located
within 50µm of bone (Fig. 3a-b). We noted that fewer cells (TUNEL+) underwent
apoptosis in this area (Fig. 3c-d) highlighting the protective effect of BDFs being
generated from bone degradation. To consider the effect of bone marrow stromal cells on
MM cells distal from bone, we performed *in vitro* experiments and found a significant
increase in the proliferation of MM cells grown in the presence of conditioned medium
from MSCs and preosteoblasts, but not osteoblasts (Fig. 3e-f). To integrate these
observations into the HCA, we assume that the intrinsic rate of MM cell division increases
with BDF and when a preosteoblast or MSC is near the MM cells (Fig. 3g-h and
Supplementary Equation 11).

Next, to study the interactions of the MM-bone marrow microenvironment in the
HCA model, we initialized each simulation with a single MM cell near a newly initiated
bone remodeling event and the formation of an osteoclast. This assumption is a
simplification of the colonization process, in which rare colonizing myeloma cells migrate
to the endosteal niche[50,51]. The HCA model revealed exciting temporal dynamics where
MM promotes successive phases of bone destruction mediated by osteoclasts that in turn
drives MM growth, thereby successfully recapitulating the vicious cycle (Supplementary
Fig. 4a and Supplementary Video 2). As expected, the mathematical model demonstrated
increasing tumor burden over time (Fig. 4a-b) with rapid loss of bone, correlating inversely
with tumor burden (Fig. 4c-d). These findings are consistent with *in vivo* data obtained
from the U266-GFP mouse model of MM which showed increasing levels of GFP positive
cells in the bone marrow following *ex vivo* flow cytometric analysis (Fig. 4e) combined
with a rapid onset of trabecular bone loss (BV/TV; Fig. 4f-g) and associated trabecular
bone parameters as assessed by high resolution μCT (Supplementary Fig. 5). The
similarities in trends between the *in vivo* model and the HCA outputs, indicated that the
HCA model was accurately recapitulating the MM-bone vicious cycle.

Furthermore, the spatial and temporal nature of the HCA allowed us to make
several observations: 1) In the model, the recruitment of MSCs *in silico* increases over
time (Fig 5a) as we and others have previously reported[52,53], 2) the model accurately
shows a suppression of adult osteoblast formation (Fig. 5b) due to inhibition of
differentiation by MM[2,54], and 3) the model predicts an early increase in preosteoblasts
followed by a reduction in numbers (Fig. 5c), consistent with previous reports[55], while
there is a concomitant increase in osteoclasts (Fig. 5d) [2,54]. We also compared these
population dynamics with our *in vivo* model. In tissue sections derived the U266-GFP
model from various time points (days 10, 40 and 100), we measured MSC, preosteoblast,
osteoblast, and osteoclast content and observed strong agreement with cell population
trends generated by the MM HCA (Fig. 5e-h and Supplementary Fig. 6). Taken together,
these data demonstrate the ability of the MM HCA to capture the vicious cycle of MM
progression in the bone microenvironment over time.

Environment-mediated drug resistance increases minimal residual disease and leads to higher relapse rates

We and others have shown that BTZ demonstrates a dose dependent cytotoxic effect on MM (Supplementary Fig. 3a)[56,57]. The compound is also effective *in vivo* but MM still grows albeit at a significantly slower rate[56]. Patients also typically become refractory to BTZ. This indicates that MM cells are 1) protected by the surrounding bone ecosystem, or 2) due to selective pressure and mutation or other mechanisms such as epigenetic changes, drug resistant clones emerge, or 3) that both ecological and evolutionary contributions can occur in parallel. Here we sought to use the spatial nature of the HCA model to gain a deeper understanding of how MM resistance evolves focusing initially on the contribution of bone ecosystem, i.e., EMDR. We confirmed the EMDR protective effect conferred by bone stromal cells on MM in the presence of BTZ *in vitro* (Fig. 6a) and integrated this effect into the HCA model (Fig. 6b). BDF was also included since it can provide a survival advantage to MM cells in the presence or absence of treatment[58,59]. Next, we initialized HCA simulations with a homogeneous sensitive MM population. BTZ was applied once the tumor burden reached a volume of 10% to mimic the scenario of diagnosis in the clinical setting. Our results show that without EMDR, BTZ completely eradicated the disease at high doses (Fig. 6d, Supplementary Fig. 3j), consistent with our *in vitro* findings. However, when EMDR effects are included in the model, BTZ reduced MM burden significantly, but the disease persisted at a stable, albeit lower, level and did not grow over time compared to existing *in vivo* data (Fig. 6c-d). These data suggest that EMDR does not directly contribute to MM relapse but does protect a small volume of MM cells from BTZ. Therefore, to address the relapse and the emergence of BTZ resistance in MM cells, we integrated a resistance probability ($p\Omega = 10^{-4}$ or $p\Omega = 10^{-3}$) during cell division, which allowed for the emergence of BTZ resistance. The probability of a MM cell to develop resistance to BTZ are estimated based on the current literature, in which mammalian cancer cells have a probability of developing resistance to numerous treatments of between 10^{-3} to 10^{-6} [60,61]. Based on our *in vitro* observations, we also incorporated a cost of resistance[62] in the model such that BTZ-resistant cells proliferate at a slower rate and are out-competed by PI-sensitive cells in the absence of treatment (Supplementary Fig. 7).

We then repeated our *in-silico* experiments and observed that with the lower resistance
probability ($p_\Omega = 10^{-4}$), EMDR increased the likelihood of tumor progression with more
simulations likely to relapse (54.4%, n = 125) compared to tumors without EMDR (6.4%,
n = 125; Fig. 6e and g; Supplementary Video 3). Similarly, with a higher resistance
probability ($p_\Omega = 10^{-3}$) tumors were more likely to relapse when EMDR is present (100%,
n = 25) compared to tumors without EMDR (56%, n = 25, Fig. 6f and h; Supplementary
Video 4). However, the higher resistance probability also increased the likelihood of tumor
progression regardless of EMDR, implying a greater role for MM intrinsic resistance
mechanisms during tumor relapse. To strengthen these findings, we tested a more
clinically relevant treatment strategy, in which BTZ therapy was pulsed (2 weeks on, 1
week off) and observed similar results (Supplementary Fig. 8). To validate our *in silico*
results, we utilized both *in vitro* and *in vivo* methodology. To this end, U266 MM cells were
cultured alone (monocultures) or with protective human MSCs (huMSCs) and exposed to
vehicle or BTZ. BTZ-treated U266 groups, responded to BTZ as evidence by a reduction
in MM confluency (Fig. 6j). However, we observed that BTZ was less efficient when U266
were cultured with huMSC and recovered over a 30-day period, whereas monocultures
did not. Further, co-cultured U266 cells treated with a second dose of BTZ, continued to
proliferate, even beyond initial confluency, and thus were considered "relapsed", whereas
this was not the case in monocultures (Fig. 6K). Since the propensity of MM cells to
develop resistance cannot be readily manipulated, we repeated the *in vitro* experiments
with a mixed population of MM cells that were either sensitive (U266; YFP positive) or
resistant (U266-PSR; RFP positive). In cultures composed of 90% PI-sensitive U266,
10% PI-resistant U266-PSR, we observed that MSCs protect against BTZ, leading to
enhanced relapse compared to MM cells cultured alone thus confirming our *in silico*
observations. Next, we investigated the role of EMDR *in vivo*. Currently, there are no
approved stromal targeting therapies available for the treatment of MM, however, Zol is
frequently given to patients to inhibit osteoclast-mediated bone destruction that in turn
also reduces the release of BDF that promote MM survival. NSG mice were inoculated
with 90% PI-sensitive U266-GFP-Luc and 10% PI-resistant-RFP MM cells. Upon
detection of the tumors in the hindlimbs, mice were divided in to two groups and
pretreated with either vehicle or Zol for one week to limit osteoclast-mediated release of

BDFs. Following pretreatment, mice were further subdivided and treated with BTZ only or BTZ and Zol for another week. As predicted by our *in-silico* results, limiting EMDR with Zol led to a deeper response to BTZ in PI-sensitive MM, as evidence by bioluminescence imaging and end point flow cytometry (Fig 6n-o).

Our HCA model revealed during BTZ application, EMDR protected a reservoir of sensitive cells that ultimately develops intrinsic resistance leading to the increased relapse rates observed (Fig. 8a-b; Supplementary Fig. 9a). The role of this sensitive reservoir in relapse is particularly evident at the lower resistance probability, where tumors with EMDR exhibited more variable (generally longer) relapse times compared to tumors without EMDR. When EMDR is absent, many tumors go extinct and relapse only occurs if intrinsic resistance arises early following treatment, whereas with EMDR, sensitive cells persist, and resistance can arise later in the course of the disease. We validated this finding *in vitro,* where we demonstrate that MSCs protect a small portion of PI-sensitive U266 MM cells from BTZ treatment, whereas in cultures containing only MM cells, PSR-RFP MM cells ultimately became the sole clone upon relapse following BTZ treatment (Fig 7c-d). Further, *in vivo*, treatment of mice with BTZ, led to the outgrowth of PI-resistant PSR-RFP. However, in Zol-pretreated (EMDR-inhibited) mice we see a deeper reduction in PI-sensitive MM cells compared to BTZ-only treated mice, where EMDR is intact (Fig. 7e-f). We next determined the clinical relevance of whether PI sensitive MM cells existed in patients that were considered to have relapsed refractory MM (RRMM). We isolated CD138+ cells from MM and exposed the cells to BTZ *ex vivo*. We observed that approximately 20% of relapsed refractory MM patients who a failed a PI-containing regimen (n=86) contained MM cells that are still sensitive to PI treatment thus supporting our *in silico* and *in vitro* and *in vivo* findings. Taken together, these results demonstrate the ability of the HCA to predict the effect of resistance and EMDR on tumor relapse and indicate a vital role of EMDR in contributing to minimal residual disease and the development of relapse refractory MM.

Environment-mediated drug resistance and resistance probability impact MM heterogeneity in relapsed disease

Even though relapsed tumors with a high resistance probability had similar growth
dynamics with and without EMDR, we noted that the composition of the tumors differed
greatly. Myeloma is a clonal disease with the prevalence of clones changing throughout
treatment[23,50,63,64]. Given the spatial resolution of the HCA model, we next asked whether
EMDR impacted the heterogeneity of resistant tumors. To this end, we tracked the
number and spatial localization of new clones forming from unique resistance events
under BTZ treatment conditions in the presence or absence of EMDR. We observed that
at a high resistance probability ($p_\Omega = 10^{-3}$) EMDR drove the evolution of significantly more
resistant subclones (mean = 5.2 subclones with >10 cells, n = 24 simulations) compared
to non-EMDR conditions where the arising population was composed largely of a single
resistant clone (mean = 1.2 subclones with >10 cells, n = 10 simulations; Fig. 8a), with
similar results at lower resistance probabilities and pulsed BTZ treatment (Supplementary
Fig. 9b-c). *In vivo*, we observed a greater reduction in the ratio of GFP+ sensitive to RFP+
resistant MM when mice were treated with Zol+BTZ compared to BTZ only (Fig 8b-c).
Moreover, the HCA revealed a significant proportion of resistant subclones originated in
close proximity to MSCs/preosteoblasts (Fig. 8d) or following release of BDF from
osteoclastic bone resorption (Supplementary Fig. 9c). Taken together, these data would
indicate that EMDR not only leads to enhanced relapse, but increased MM heterogeneity
due to the emergence of independent resistant MM clones. Further, it is also plausible
that EMDR may give rise to MM clones with potentially unique intrinsic BTZ resistance
mechanisms making the treatment of relapsed tumors more challenging. Together, these
data support that early targeting of bone marrow microenvironment, and thus EMDR,
would lead to reduced MM heterogeneity and potentially deeper responses with
subsequent lines of treatments.
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Discussion
Understanding the factors that govern the evolution of refractory MM remains of huge
clinical importance. Dissecting how intrinsic and bone ecosystem mechanisms contribute
to the evolution of the disease in the presence or absence of treatment or where these
clones arise spatially are difficult questions to address with standard experimental
techniques alone. Here, we address this using a novel experimentally derived hybrid

cellular automaton (HCA) model of MM evolution in the bone ecosystem that provides

new insights. For example, we show that the bone ecosystem contributes to minimal

residual disease, and MM clonal heterogeneity. These findings are in part supported by

previous studies revealing enrichment of binding proteins and chemokine receptors on

MM cells in minimal residual disease, indicating a likely role for stromal interactions in

facilitating relapse[65]. Our findings and additional wider biological validation provide

rationale for the targeting of the bone ecosystem during the application of standard of

care treatment to prevent the emergence of multiple resistant clones.

Our own *in vitro* and *in vivo* data, as well as data from the literature, were used

where possible to parameterize and calibrate the HCA model. However, there were some

parameters that could not be estimated, and the specific assumptions that have been

incorporated into the HCA may impact the generality of the results. For example, we

assume that MSCs are recruited in proportion to tumor burden based on experimental

data in non-treatment conditions, but the application of treatment could alter this

recruitment rate and thus bone ecosystem protective effects. Furthermore, there are

limitations to how well parameters estimated from *in vitro* data correspond to the *in vivo*

setting. To address this, we tested the robustness of the model results by varying a subset

of parameter values to determine the impact on simulation results (Supplementary

Methods 1.4; Supplementary Fig. 10). Overall, our finding that EMDR increases minimal

residual disease and leads to higher relapse rates was consistent across parameter

values, underscoring the robustness of the model.

There have been several mathematical models that explore interactions between

MM and the bone marrow microenvironment. For example, ordinary differential equation

(ODE), evolutionary game theory (EGT), and hybrid agent-based models have revealed

insights into MM growth in bone and have even taken into consideration the impact of

MM progression on bone destruction[66-72]. Additionally, mathematical models have

focused on how ecosystem effects contribute to drug resistance[73-76]. However, the HCA

model presented herein represents a significant advance in that it is carefully integrated

with biological data to recapitulate the bone-MM ecosystem under normal and treatment

conditions and is the first model to dissect intrinsic vs. ecosystem driven resistance in

multiple myeloma. A major additional advantage of our model is its spatial nature, allowing

us to visualize and measure where the ecosystem, and particularly stromal cells,
contribute to the generation of resistant clones.

Our model shows that resistant MM clones can arise independently of the bone
ecosystem during BTZ treatment if the resistance probability is sufficiently high. But, when
EMDR is present, we observe the evolution of higher numbers of resistant clones near
MSCs/preosteoblasts/BDF during continuous BTZ treatment. The model also suggests
that targeting of EMDR during treatment would reduce MM heterogeneity. Various
adhesion molecules and cytokines such as the CXCL12/CXCR4 and IL-6/JAK/STAT axis
have been shown to mediate ecosystem protective effects and drugs/biologics that
specifically target those pathways have been trialed[77,78]. Unfortunately, these drugs have
had little success translating to clinical practice due to limited survival improvements when
added to existing therapies[79], thus there remains a need to identify multiple mechanisms
of EMDR in patients with novel therapies and feasible methods of delivering these drugs.
However, we posit that early intervention with EMDR-targeting agents, perhaps in
combination, would reduce tumor heterogeneity, rendering relapsing tumors vulnerable
to a targeted second line therapy that targets the predominantly homogenous disease.
As such, future studies/trials should take into consideration the tumor diversity upon
relapse and response to second line therapies.

Another important aspect of the model is the ability to apply and withdraw therapy
at varying stages of MM progression to quantitatively determine the impact on MM over
time which may be useful for adaptive therapy design and implementation. Adaptive
therapy is an emerging, evolution-inspired approach for cancer treatment that exploits
competitive interactions between drug sensitive and drug resistant cells to maintain a
stable tumor burden[62]. Several models have studied the many ways therapies can be
applied in an adaptive manner ensuring that the competition between treatment resistant
and naïve populations allows for better overall survival for cancer patients. Importantly,
our model captures tumor interactions with the bone ecosystem and thus includes the
potential impact of the bone ecosystem on adaptive therapy. This allows us to study not
only how treatments impact tumor populations but also their influence on bone ecosystem
cells such as osteoblasts and osteoclasts, and how this can then influence MM response
since the protective bone microenvironment can serve as a reservoir of sensitive cells

under treatment. Clinical trials thus far using adaptive therapy guided by mathematical
modeling have had encouraging results. For instance, recent studies have shown that in
patients with bone metastatic prostate cancer, adaptive therapies guided by mathematical
models can increase the time to progression and the overall survival using standard of
care treatments[80]. These data support the feasibility of integrating mathematical modeling
for the design of patient specific treatment. It should be noted however, the HCA model
is parameterized with a variety of in vitro, in vivo, and human data, making translation
directly to the clinic challenging in its current form. This can be resolved with further
rigorous model calibration and validation using clinical data, and multiple efforts at moving
agent-based models into the clinical setting are underway[29-31,81,82].

A key component of our HCA model lies in its ability to recapitulate the homeostatic
nature of bone remodeling over prolonged periods (~4 years). As we demonstrated, the
impact of therapies on tumor-naïve bone volume and the bone stromal cellular
components that control the process can also be quantitatively examined. It also can
examine non-cancerous bone diseases that result from an imbalance in bone remodeling
such as osteoporosis[83]. The underlying causes of osteoporosis can result in differing
effects on osteoclasts and osteoblasts, which could be incorporated into the model. For
example, estrogen deficiency increases the lifespan of osteoclasts while having the
opposite effect on osteoblasts, whereas age-related senescence is characterized by
decreased osteoclastogenesis and osteoblastogenesis[83]. Osteoporosis treatments
include anti-resorptive therapies (e.g., bisphosphonates) and bone formation therapies
(e.g., intermittent PTH). By modifying certain model parameters, we can explore the effect
of different therapeutic strategies on disease outcomes to determine if certain treatments
are more effective in particular scenarios[84]. While we have primarily used Zol and BTZ
for proof of principle, the model can be easily adapted to integrate the effects of other
standard of care therapies as single agents or in combination such as dexamethasone,
and IMIDs. Importantly, the temporal and cellular resolution of the model also can identify
key moments in which to administer treatments to maintain a healthy bone volume.

Our HCA model, like all models, has caveats. For example, its two-dimensional
nature does not take into account the potential three-dimensional role in evolutionary
dynamics[85,86] or the vascular nature of the bone marrow-MM microenvironment that can

play a role in drug/nutrient diffusion,[10,87]. However, these can be incorporated into the

model, if necessary, upon availability of relevant experimental data. Another potential and

future extension of the model is to incorporate the immune ecosystem given its role in

controlling bone turnover and cancer progression[10,87], the influence of BDFs on immune

populations[88,89] and the growing armamentarium of immunotherapies in MM. Here, we

excluded the immune component to focus solely on the role of the bone stroma on MM

progression combined with the fact that MM growth in immunocompromised mice was

used to parameterize and compare model outputs. Infiltrating immune cells have noted

effects on cancer progression. For example, initially, natural killer (NK) cells and cytotoxic

T lymphocytes can drive an anti-tumor response[90]. However, as the tumor progresses,

immunosuppressive populations expand including myeloid derived suppressor cells

(MDSCs) and regulatory T-cells (Tregs)[90]. MM is characterized by an increase of inactive

NK cells, MDSCs, and Tregs and treatments such as bortezomib can alter the

composition and activity of infiltrating or resident immune cells[90,91]. Tumor-immune

dynamics in MM have been previously explored with ODE models[92,93] and parameters

derived from *in vitro* or *in vivo* studies can be integrated into our HCA model albeit with a

limit on complexity. Another caveat is the difficulty in determining the rate of MM

resistance and the assumption that it occurs intrinsically due to treatment pressure. Prior

studies suggest that drug resistance may arise through the selective expansion of pre-

existent resistant tumor cells, *de novo*, or through the gradual increase in resistance over

time[94]. In our model, we assume that after treatment initiates (i.e., once the bone marrow

consists of 10% of MM cells), there is a probability that a dividing MM cell could develop

a resistance mechanism, and that mechanisms directly causes resistance to bortezomib

resulting in heterogeneity. This resistance probability that would lead to treatment

resistance is difficult to assess in patients or in experimental models but the resultant

heterogeneity arising from different resistance probabilities may allow us to infer

resistance rates in patients. Moreover, the *in silico* model is not fixated on specific

resistance mechanisms currently but more on whether a cell is sensitive or not. One such

benefit of the *in silico* model is the ability to alter parameters, such as p_Ω, response to

treatment and doubling time, to mimic the heterogeneity seen in the clinic.

In conclusion, we have described a new mathematical model of MM evolution in

the context of the bone ecosystem. Our results show that, under treatment conditions, the

interactions between the bone ecosystem and the tumor contributes to the presence of

residual disease and to the enrichment of tumor heterogeneity. These results suggest

that early intervention with drugs that target the bone ecosystem could lead to MM

extinction or at the very least reduce tumor heterogeneity by preventing the evolution of

multiple drug resistant clones. Given the current interest in novel strategies of treatment

that consider the evolutionary dynamics in cancer such as adaptative therapies, we also

predict that our model can be a useful clinical tool in guiding patient specific treatment

strategies.

Methods

Hybrid Cellular Automaton Model

The model we developed builds on the HCA paradigm first described by Anderson *et al.*

and used to study evolutionary dynamics in cancer and our work in the context of bone

metastasis[41-43,95,96]. By definition, an HCA consists of discrete cell types that are updated

once per time step according to a set of flow charts (Fig. 1c) as well as a set of partial

differential equations that describe cytokines in the microenvironment. Here, we consider

six different cell types, including precursor osteoclasts, active osteoclasts, mesenchymal

stem cells (MSCs), precursor osteoblasts, active osteoblasts, and multiple myeloma cells.

Additionally, we incorporate two signaling molecules including RANKL and bone derived

factors (BDFs) such as transforming growth factor beta (TGF-β). In the sections below,

we describe the interactions between cell types and cytokines that are key in bone

remodeling and MM progression. Further details can be found in Supplementary Methods

1.

Parameters and grid

We implemented our model using the Hybrid Automata Library (HAL)[97]. When possible,

parameters for the HCA model were derived from empirical and published data

(Supplementary Tables 1-6). The model is defined on a 2D rectangular grid (160 x 150

pixels) representing a $1600 \times 1500 \ \mu m^2$ cross section of the bone marrow. Trabecular

bone is defined in the center of the grid and initially consists of 12.9% of the total area,

consistent with our *in vivo* data (Supplementary Methods 1.1). Normal bone remodeling events are uniformly distributed over 4 years, the approximate turnover time of trabecular bone[83]. A remodeling event is initiated by the expression of RANKL by five osteoblast lineage cells on the perimeter of the bone.

Preosteoclasts and osteoclasts

Precursor osteoclasts follow the gradient of RANKL to the bone remodeling site. With a given probability, at least five preosteoclasts will fuse together to become a multinucleated osteoclast. Active osteoclasts resorb bone matrix, leading to the release of BDF. We assume that the amount of bone that osteoclasts resorb is proportional to their lifespan of approximately 14 days[83,98].

MSCs, preosteoblasts, and osteoblasts

After an osteoclast fuses, an MSC is placed on the grid within a radius of $40\ \mu m$ of the osteoclast, provided there is not already an MSC within the neighborhood. This requirement ensures that MSCs are located adjacent to sites of bone remodeling and can couple bone resorption with bone formation[36]. MSCs undergo asymmetrical division to create preosteoblasts, which proliferate when BDF is above a certain threshold or differentiate into bone matrix-producing osteoblasts when BDF is below the threshold (Supplementary Fig. 2c). We assume that osteoblast lifespan is proportional to the amount of bone that was resorbed at the location of the osteoblast, which is approximately 3 months. In the model, we assume that osteoblast death is proportional to the amount of bone that was resorbed by the osteoclast subunit that had occupied the space. Whilst this is a simplifying assumption of the biology, this assumption permits the coupling of bone resorption with bone formation, since the lifespan of an osteoblast controls how much bone the osteoblast forms. Bone resorption and bone formation are tightly coupled processes[99]. The definitive mechanisms through which osteoclasts and osteoblasts sense each other and their catabolic/anabolic processes have still not been fully elucidated and can be context dependent. However, several mechanisms are known to play a role including the release of bone derived factors (BDFs; namely TGF-beta and IGF-1), osteoclast derived factors such as sphingosine 1-phosphate, extracellular vesicles, apoptotic bodies containing RANK, and demineralized collagen remnants in the resorption lacunae. To model each of these mechanisms independently would make our

model very complex as well as computationally expensive. We therefore integrated a
straightforward coupling of osteoblasts and osteoclasts in the model. Further, when an
osteoblast is buried, this has consequences for bone homeostasis. To maintain a steady
state of bone, the lifespan of the nearest osteoblast is increased to allow it to build more
bone to compensate for the amount lost due to the buried osteoblast. Whilst this is a
simplifying assumption, research suggests osteoblast lineage cells communicate through
gap junctions. This allows osteoblasts to coordinate activities and ensure new bone tissue
is deposited at the correct location and in the appropriate amount to maintain structural
integrity and bone homeostasis[100-104].

Cytokines

RANKL (R_L) and BDF (T_β) are two key cytokines that drive the normal bone remodeling
process. RANKL is produced by osteoblast lineage cells ($\alpha_R B_{i,j}$) with natural decay of the
ligand ($\delta_R R_L$). BDF is released during bone resorption ($\alpha_T B_{i,j} C_{i,j}$) with natural decay of
the ligand ($\delta_T T_\beta$). We also assume that there is a constant production of BDFs (α_B) by
other cell types that are not explicitly defined in the model. These cytokines are
incorporated into our model through the following system of partial differential equations
(PDEs):

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$$\frac{\partial R_L(x,y,t)}{\partial t} = \underbrace{D_R \left(\frac{\partial^2 R_L}{\partial x^2} + \frac{\partial^2 R_L}{\partial y^2} \right)}_{\text{Diffusion}} + \underbrace{\alpha_R B_{i,j}}_{\text{Production}} - \underbrace{\delta_R R_L}_{\text{Decay}}$$

$$\frac{\partial T_\beta(x,y,t)}{\partial t} = \underbrace{D_T \left(\frac{\partial^2 T_\beta}{\partial x^2} + \frac{\partial^2 T_\beta}{\partial y^2} \right)}_{\text{Diffusion}} + \underbrace{\alpha_B}_{\substack{\text{Basal} \\ \text{Production}}} + \underbrace{\alpha_T B_{i,j} C_{i,j}}_{\text{Production}} - \underbrace{\delta_T T_\beta}_{\text{Decay}}$$

where the subscripts specify the location on the grid, i.e., $x = ih$, $y = jh$ where $\{i, j\}$ are
positive integers and h denotes the spatial step, $h = \Delta x = \Delta y$. The system of PDEs is
solved using the forward time centered space (FTCS) scheme with periodic boundary
conditions imposed on all sides of the domain, which is implemented using the diffusion
function in HAL.

Multiple Myeloma

A single myeloma cell is recruited within a radius of $40 \ \mu$m of an osteoclast after the first
osteoclast fusion event occurs (Fig. 4a). MM cells move and proliferate in response to

BDF and have a further proliferative advantage if they are within a radius of $20\ \mu m$ of an

MSC or preosteoblast (Fig. 3g), and a survival advantage if BDF is above a certain

threshold (Fig. 3h). As the MM cell population increases, additional MSCs are recruited.

Furthermore, if three or more myeloma cells are located close to bone, a new bone

remodeling event is initiated which increases RANKL and osteoclast formation. MM cells

also prevent the differentiation of preosteoblasts if they are located within a radius of

$80\ \mu m$ of a MM cell which decreases osteoblast activity.

Treatment

The HCA incorporates the direct and indirect effects of bortezomib by including the

cytotoxic effect on MM cells as well as its ability to inhibit preosteoclast fusion and

enhance bone formation[48,49] (Supplementary Fig. 3). To mimic the clinical scenario of MM

diagnosis, once MM reaches 10% of the bone marrow area *in silico*, treatment is applied

either continuously (as for mouse models of multiple myeloma) or pulsed (2 weeks on, 1

week off; as is performed in the clinic) until MM burden reaches 20% of the bone marrow.

In these simulations, once treatment is initiated, myeloma cells have a probability of

developing resistance mechanisms during cell division that would cause the MM cells to

become resistant to bortezomib. MM cells that are within a radius of $20\ \mu m$ of an MSC or

preosteoblast or are located at a position where BDF is above a certain threshold, have

a survival advantage during treatment referred to as environment mediated drug

resistance (EMDR).

Multiple myeloma mouse models

All animal experiments were performed with University of South Florida (Tampa, FL)

Institutional Animal Care and Use Committee approval (CCL; #7356R). Male and female

14–16-week-old immunodeficient mice NOD-SCIDγ (NSG) mice were divided into tumor

naïve or tumor bearing mice GFP-expressing human U266 (U266-GFP) multiple

myeloma cells were injected (5×10^6 cells/100μL PBS) or PBS (100μL) via tail vein. Mice

were euthanized at days 3, 10, 20, 40 and 100 (3-5/group/timepoint). In a separate

experiment male and female 8 week-old NSG mice were inoculated with PI-sensitive

U266-GFP-Luc (90%) and PI-resistant PSR-RFP (10%) MM cells via tail vein injection

(5×10^6 cells/100μL PBS). Upon detection of tumor burden in the hind limbs via

bioluminescent imaging (IVIS), mice were randomized to two groups to receive either
twice weekly vehicle (PBS) or Zol (30μg/kg). Following one week of Zol pretreatment,
mice were further randomized in to four subgroups and received the following: Group 1
Vehicle (5 mice), Group 2 Zol (30μg/kg/twice weekly; 5 mice), Group 3 Zol+BTZ (7 mice),
Group 4 BTZ (0.5mg/kg/twice weekly; 4 mice). After one week of BTZ treatment, all mice
were euthanized. Tibiae were excised and soft tissue removed for histological and FACs
analyses.

Micro-computed Tomography, Immunofluorescence and Histomorphometry,
Harvested right tibiae were fixed in 4% paraformaldehyde (PFA) in 1x phosphate buffered
saline (PBS) for 48 hours at room temperature. Evaluation of trabecular bone
microarchitecture was performed in a region of 1000 μm, beginning 500μm from the
growth plate using the SCANCO μ35CT scanner. Tibiae were decalcified in an excess of
10% EDTA at pH 7.4 at 4°C for up to three weeks with changes every 3 days before being
place in cryoprotection buffer (30% sucrose), frozen in cryomedium (OCT) and subjected
to cryosectioning to yield 20 μm tissue sections. Sections were dried, washed and blocked
before addition of primary antibodies (anti-pHH3; 06-570 Millipore, anti-Osterix; ab22552,
abcam: anti-αSMA: PA5-16697, Invitrogen). Slides were washed and incubated with
goat anti-rabbit Alexa Fluor-647-conjugated secondary antibody and counterstained with
DAPI. Mounted sections were imaged using 10X image tile-scans of whole tibia. pHH3+,
αSMA+, Osterix+ or GFP+ cells were identified and quantified using Fiji software[105]. Dual
ALP and TRAcP staining were performed on cryosections. Brightfield visualization was
performed using the EVOS auto at 20X magnification. Five images per section were taken
and the number of ALP+ cuboidal bone-lining osteoblasts and red multinucleated
TRAcP+ osteoclasts per bone surface were calculated.
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619 *For additional and in-depth methods, please see supplementary materials.*
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Author Contributions
A.K.M and D.B. were responsible for computational model design and execution. R.T.B
and C.C.L were responsible for biological experimentation design and analysis**.** T.L, N.N,

J.F performed biological experiments. P.R.S, R.C, A.S and K.H.S were involved in

conception, design, experimentation, and analysis of *ex vivo* samples. A.K.M, R.T.B,

C.C.L and D.B were involved in overall concept and design. All authors were involved in

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Data availability statement

All the data supporting the findings of this study are available within the article and its

Supplementary information files and from the corresponding author upon reasonable

request. A reporting summary for this article is available as a Supplementary Information

file. Source data are provided with this paper.

Code availability statement

The code generated in this manuscript is available at

https://github.com/dbasanta/MM_ABM

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Figures

Fig. 1. Development of a hybrid HCA of the naïve and myeloma bone
microenvironment.

a, Bone-lining osteoblast lineage cells release RANKL inducing fusion and maturation of
osteoclasts (1). Osteoclasts resorb the bone, releasing stored bone-derived factors
(BDFs) such as TGF-β (2). TGF-β recruits local MSCs and stimulates asymmetric division
in to preosteoblasts (2). When TGF-β levels remain high, preosteoblasts rapidly
proliferate. Following osteoclast apoptosis, release of TGF-β falls and preosteoblasts
differentiate to mature bone producing osteoblasts (3). While TGF-β levels remain low,
osteoblasts produce new bone (4). As bone returns to normal, a fraction of the osteoblasts
is buried within the matrix becoming terminally differentiated osteoblasts (5), the

remaining osteoblasts undergo apoptosis, or become quiescent bone-lining cells (6).

Myeloma cells enhance the formation of osteoclasts (7), enhanced bone resorption

produces higher levels of BDFs which fuel myeloma growth (8) and inhibit osteoblast

differentiation (8) and activity (9). Created with biorender.com

b, Interaction diagram between cell types in the HCA and factors such as BDFs and

RANKL (created with biorender.com). A more detailed interaction diagram with

references can be found in supplementary figure 1.

c, Flowcharts describing the sequence of steps followed by preosteoclasts, osteoclasts,

MSCs, preosteoblasts, osteoblasts, and myeloma cells.

Fig. 2. The HCA model captures all stages of bone homeostasis.

a, Images from simulations at initial conditions (left) and after 4 years (right). Legend

depicts colors of cell types in the model.

b, BMU is initiated in response to release of RANKL from bone lining cells (1).

preosteoclasts migrate to RANKL and fuse to form an osteoclast under highest

concentrations (2). osteoclast resorbs bone and stored BDFs are released which recruits

MSCs. MSCs divide asymmetrically producing preosteoblasts which proliferate rapidly

under high TGF-β conditions. Upon completion of resorption, BDF levels fall allowing for

preosteoblast differentiation to osteoblasts. osteoblasts form new bone (4) and ultimately

undergo apoptosis or become quiescent bone lining cells (5).

Fig. 3. Multiple myeloma cells receive proliferative and survival advantages from the bone marrow microenvironment.

a, Quantification of the distance of phosphorylated histone H3 positive (pHH3+; red) myeloma cells (green) to the nearest trabecular or cortical bone in U266^{GFP}-bearing mice 100 days post inoculation. N=5 tibia.

b, Representative images from experiment in **a**, DAPI (blue) was used as a nuclear counterstain. White dotted line indicates tumor bone interface. Scale bar, 50 microns.

c, Quantification of the distance of TUNEL+ (red) myeloma cells (green) to the nearest trabecular or cortical bone in U266^{GFP}-bearing mice 100 days post inoculation. N=5 tibia

d, Representative image from experiment described in **c**, DAPI (blue) was used as a nuclear counterstain. White dotted line indicates tumor bone interface. Scale bar, 50 microns.

e, Images of huMSCs differentiated to different stages of the osteoblast lineage. Cells were stained with Alizarin Red to identify mineralization.

f, Proliferation index of CM-DiL stained U266 cells 7 days after growth in 50% conditioned medium from control wells or cells of the osteoblast lineage. Results are displayed as means of at least 3 experiments.

g, Plot of functional form used to represent the division rate of myeloma cells in the presence and absence of preosteoblasts/MSCs.

h, Plot of functional form used to represent the death of myeloma cells when BDF is above and below a threshold.

* p-value < 0.05, ** p-value <0.01

Fig. 4. Computational and biological model outputs of myeloma growth and bone dynamics.

a, HCA model images showing single myeloma cell (Day 5), colonization of the marrow by MM cells (Day 75), increased osteoclastogenesis (Day 75, RANKL), bone resorption

(Day 75; BDF) and eventual takeover of the marrow by MM cells (Day 350). Light green

myeloma cells indicate MM cells with proliferative or survival advantage.

b, Myeloma growth dynamics in HCA model in the absence of treatment.

c, Myeloma induced loss of trabecular bone in HCA model compared to normal bone

homeostasis.

d, Bone loss decreases rapidly with myeloma expansion *in silico*.

e, Myeloma growth in bone marrow of mice inoculated with U266-GFP cells over time

N=3-5 tibia per time point.

f, Trabecular bone volume fraction (BV/TV) was assessed *ex vivo* with high-resolution

microCT. N=3-5 tibia per time point.

g, Biological model shows rapid myeloma-induced bone loss.

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Fig. 5. Computational and biological model outputs of cell types in the myeloma bone microenvironment. **a-d,** Computational model outputs of increasing MSC percentage of the marrow area (%MA) (**a**), loss of osteoblasts (**b**) rise and fall of preosteoblast percentage (**c**) and increasing osteoclast percentage due to growth of MM (**d**). **e-h**, *Ex vivo* analysis of histological sections from the U266-GFP myeloma model (N=3-5 tibia per time point.) per time point demonstrates increasing presence of αSMA+ MSCs (**e**), loss of ALP+ cuboidal osteoblasts (**f**), early increase and subsequent reduction of OSX+ preosteoblasts (**g**) and increasing numbers of TRAcP+ multinucleated osteoclasts (**h**) compared to tumor naïve mice.

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Fig. 6. EMDR contributes to minimal residual disease and relapse.

a, GFP+ U266 MM were plated alone or with huMSCs in the presence or absence of BTZ; MM burden was measured after 72h by area covered by GFP+ cells.

b, Interaction diagram showing the cell types and factors in the HCA that are affected by BTZ or contribute to EMDR.

c, *In vivo* growth of MM cells with and without BTZ treatment, data was taken from [42].

d-f, Model outputs of MM growth with continuous BTZ treatment, +/- EMDR when MM cells do not develop resistance (**d**) or with a probability to develop resistance (10^{-4}, **e** or 10^{-3}, **f**) and develop resistance.

g-i, Kaplan-Meier plot of relapse-free survival from simulations described in **d-f**.

j, Nuclear-eYFP+ U266 were cultured alone or with huMSCs in the presence or absence of 10nM of BTZ. MM growth was tracked by eYFP over 60 days. Yellow shading indicates periods when treatment was on.

k, Kaplan-Meier plot of 'relapse' (wells reaching >20% MM confluency) from experiment described in j.

l, MM cells (90% U266- Nuclear-eYFP+ and 10% PSR-RFP+) were cultured alone or with huMSCs in the presence or absence of 10nM of BTZ.

m, Kaplan-Meier plot of 'relapse' (wells reaching >20% MM confluency) from experiment described in l.

n, Average U266 growth by BLI after MM cells (90% U266-GFP$^+$Luc$^+$, 10% PSR-RFP) were tail vein injected into NSG mice. Mice were divided into two groups and pre-treated with vehicle or Zol (30ug/kg) for 1 week prior to mice being randomized and treated with either vehicle (n=5 mice), Zol (n=5 mice), Zol+BTZ (n=7 mice), or BTZ (0.5mg/kg; n= 4 mice). Pink and green arrows indicate days of Zol or BTZ treatment respectively.

o, Representative BLI IVIS images from the experiment described in **n**.

Fig. 7. EMDR contributes protection of sensitive MM and tumor heterogeneity.

a, HCA images from simulations with continuous BTZ application, with no resistance probability ($p_\Omega=0$) or high resistance probability ($p_\Omega=10^{-3}$) in the presence or absence of EMDR.

b, Computational outputs of the proportion of BTZ-sensitive and BTZ-resistant MM cells 1 year on treatment (left) and at relapse (right) with $p_\Omega=10^{-3}$. Related to Figures 6f and 6i.

c, Representative images of U266-nuclear eYFP+ and PSR-RFP+ cells at relapse when cultured alone or huMSCs, with or without BTZ in vitro. Related to figure **6j-k**.

d, The proportion of BTZ-sensitive (U266-nuclear eYFP+) and BTZ-resistant (PSR-RFP+ MM cells cultured alone or with huMSCs with and without BTZ on treatment (left) and at relapse (right). Related to Figures **6l-m** and **7d**.

e, Representative flow plots of BTZ-sensitive (U266 GFP+Luc+; green) and BTZ-resistant (PSR-RFP+; black) from the bone marrow (gray) of NSG mice treated with vehicle, Zol, Zol+BTZ or BTZ. Vehicle = 10 femur, Zol = 10 femur, Zol+BTZ = 12 femur, BTZ = 8 femur.

F, Proportion of BTZ-sensitive (U266 GFP+Luc+) and BTZ-resistant (PSR-RFP+) MM cells in the bone marrow of NSG mice treated with vehicle, Zol, Zol+BTZ or BTZ.

g, schematic of the EMMA platform. CD138+ MM cells and stroma are isolated from MM patients and co-cultured without test compounds. Live cell imaging is used to assess viability.

h, The AUC of MM cells from RRMM patients, whose last relapse was to a PI-containing regimen (PI) or a non-PI containing regimen (Other), in response to BTZ. Green dots identify sensitive MM cells (quartile 1).

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Fig. 8. EMDR contributes to tumor heterogeneity upon relapse.

a, Muller plots of sensitive and individual BTZ resistant (Res) sub-clones from simulations

described in **a-c**. Colors denote different subclones. Red arrow indicates start of BTZ

treatment. **** pvalue <0.0001

b, Images of GFP+ U266 (green) and RFP+ PSR (red) MM cells and cell nuclei (DAPI;

blue) in tibial sections of mice from *in vivo* study described in Figure 7. Magnification 20X.

Scale bar 50 microns.

c, Relative quantification of GFP+ U266 and PSR MM in tibial sections described in Figure

8b. Vehicle = 5 tibia, Zol = 5 tibia, Zol+BTZ = 7 tibia, BTZ = 4 tibia.

d, Mean number of resistant sub-clones arising following BTZ treatment tumors that

reached 20% with resistant subclones and the locations within the bone marrow

microenvironment where each subclone originated, with/without EMDR from simulations

described in **a**. n = 13/25 (No Treatment), n = 10/25 (No EMDR+BTZ), n = 24/25

(EMDR+BTZ).

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Supplementary: The bone ecosystem facilitates multiple myeloma relapse and the evolution of heterogeneous proteasome inhibitor resistant disease.

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Supplementary Methods

1. Hybrid Cellular Automaton Methods

We developed a new hybrid cellular automaton (HCA) model to capture some of the key cellular and molecular populations that characterize the MM bone ecosystem. This model was developed from scratch although some of the assumptions, including those about what are the most important populations for the model, build on our previous experience building a similar model to study bone metastatic prostate cancer[1-3]. In this instance our code (available on this repository: https://github.com/dbasanta/MM_ABM) build on the HAL library which will help our code become a more self-sufficient and reusable platform of use to other bone-modelling scientists. We have generated different and novel data and *in vivo* model to parameterize, calibrate the model and validate the results. Building on our experience starting computational models of cancer from homeostasis, this new code is more robust and capable of performing bone remodeling simultaneously in several sites. This robustness is also demonstrated by the fact that homeostasis in the bone is preserved even with the use of variable depths of osteoclast-mediated bone resorption which was not the case previously.

The model we developed incorporates six different cell types, including precursor osteoclasts, active osteoclasts, mesenchymal stem cells (MSCs), precursor osteoblasts adult osteoblasts, and multiple myeloma (MM) cells. Additionally, we incorporate two signaling molecules including RANKL and bone derived factors (BDFs) such as transforming growth factor beta (TGF-β). In the sections below, we describe the specific assumptions and parameters incorporated into the HCA of normal bone remodeling (**Supplementary Section 1.1**), multiple myeloma (**Supplementary Section 1.2**), and bortezomib treatment (**Supplementary Section 1.3**). Refer to **Supplementary Tables 1-6** in **Supplementary Section 1.5** for a complete description of the parameters and values used in the HCA.

1.1. Normal Bone Remodeling

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Algorithmic Implementation

Initial and boundary conditions of agent grid

We first develop a model of trabecular bone remodeling in which we represent a cross section of the bone marrow as a 2D rectangular grid. We define the length of the grid as $0 \leq x \leq 160\,px$ and the height as $0 \leq y \leq 150\,px$, where $\Delta x = 1\,px = 10\,\mu m$, the diameter of a myeloma cell. To obtain the initial arrangement of bone, we first initiated the bone as a $60\,px \times 50\,px$ rectangle in the center of the grid, surrounded by bone marrow. The initial area of the bone was set to represent the approximate bone area to total area (BA/TA) from sham limbs of wild type RAG2 mice (mean: 12.4%, n = 6, data not shown). As bone remodeling occurs over time, the initial rectangle is transformed, though the BA/TA remains approximately constant. We arbitrarily select one of these final bone configurations as the initial condition for subsequent runs of the model. Hence, trabecular bone initially consists of 12.9% of the total area. We assume that the number of precursor osteoclasts remains constant and is approximately equal to the number of monocytes, which is 2.8% of the bone marrow[4]. MSCs initially consist of 0.01% of the bone marrow[5]. We implement periodic boundary conditions on all sides of the domain for all cell types.

Timesteps

We use two separate time step sizes, Δt_{diff} and Δt_{cells}, to account for the differences in the timescales for diffusion (fast) versus cell processes (slow). We use $\Delta t_{diff} = 1\,sec$ and $\Delta t_{cells} = 6\,min$.

Simulation Process

The computational algorithm was implemented using the Hybrid Automata Library (HAL)[6] and is organized as shown in **Supplementary Fig. 1a** and **Fig. 1c**.

Precursor osteoclasts

Fusion

Precursor osteoclasts fuse and become multinucleated osteoclasts. This process is
regulated by the expression of RANKL (**Supplementary Fig. 2f**), which is expressed by
osteoblast lineage cells such as osteoblast precursors, osteocytes, and bone lining
cells[7,8]. It is not well understood which cell type is the primary source of RANKL for
osteoclast fusion, but it has been suggested that microdamage to trabecular bone leads
to osteocyte apoptosis, which may signal to bone lining cells to express RANKL[7,8]. In our
model, we assume that bone remodeling events are initiated through microfractures that
are uniformly distributed over 4 years, the approximate turnover time of trabecular bone[9].
The total number of remodeling events was approximated using the initial total amount of
bone divided by the approximate amount of bone resorbed per osteoclast. For simplicity,
each basic multicellular unit (BMU) initiates from a single remodeling event that consists
of five adjacent cells on the perimeter of bone that begin to express RANKL. The number
of cells expressing RANKL was selected to equal the approximate diameter of an
osteoclast, which is $50\,\mu m$[10].Precursor osteoclasts follow the gradient of RANKL and
once there are five adjacent cells on the perimeter of bone, they fuse to become an active
osteoclast (osteoclast) with probability

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$$p_{fusion} = 1 - (1 - MAX\_FUSION\_RATE)^{TIMESTEP\_AGENT} \#(1)$$

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This probability reflects that fusion is a process that takes at least 3 days to complete. We
note that this probability is scaled geometrically since the agent time step (6 min) is
smaller than the unit of time (1 hour), hence the probability that the preosteoclast does
not fuse per agent time step must be considered. Additionally, fusion requires stimulation
with RANKL which is modeled as a Hill function such that the probability of fusion
increases and saturates at one as RANKL increases (**Supplementary Fig. 2g**):

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$$f_{fusion}(RANKL) = \frac{1}{1 + \left(\frac{K_{aOC}}{RANKL}\right)} \#(2)$$

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A Hill function is chosen as the functional form because it is commonly used to represent
cell responses that are dependent on receptor-ligand interactions[11]. After the

preosteoclasts fuse to become an osteoclast, five new preosteoclasts are randomly

placed on the grid so that the number of preosteoclasts remains constant over time. To

assess whether these functional forms qualitatively capture the dynamics of fusion in

response to different concentrations of RANKL, we inhibit RANKL production by

multiplying the production rate by scale factor π_{Ri} (**Equation 10**). As expected, the total

number of osteoclasts decreases as RANKL decreases (**Supplementary Fig. 2h**).

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Movement

Precursor osteoclasts migrate in response to a gradient of RANKL[12,13]. We use the same

technique to describe the probability of a cell remaining stationary or moving up, down,

left, or right used in the original implementation of the hybrid discrete-continuum model[14]

(**Equation 9**). If a preosteoclast would otherwise move in a direction that is occupied by

a myeloma cell or precursor osteoblast, the two cells swap positions on the grid. This

requirement underlies the assumption that fusion is not limited by spatial restrictions and

is necessary in order to capture *in vivo* data showing that osteoclasts increase over time

due to multiple myeloma.

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Active osteoclasts

In the model, active osteoclasts consist of 5 subunits to represent the size difference

between osteoclasts and other cell types and to account for the fact that they are the

result of the fusion of 5 preosteoclasts. In order for the osteoclast to function as a single

unit, once a subunit of an osteoclast is selected for a given timestep, all of the other

subunits are collected and the action for each is defined to be the same for a given

osteoclast.

1236

1237 *osteoclast lifespan*

1238 We assume that the amount of bone that osteoclasts resorb is proportional to their

1239 lifespan, which we define to be normally distributed with a mean lifespan of 14 days[9],

1240 bounded between 7 and 21 days:

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1242 $$N(\mu_{OC}, \sigma_{OC}^2) \ within \ the \ interval \ (OC_{min}, OC_{max}) \#(3)$$

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To verify the implementation of this assumption in the model, we show that the average

osteoclast lifespan per year remains constant over time (**Supplementary Fig. 1e**). The

end of the bone resorption phase is followed by a reversal period, which couples bone

resorption and bone formation. When an osteoclast dies, it is removed from the grid, and

the cleared space is designated as eroded bone. Bone derived factors continue to be

produced at a lower level for three days, which allows precursor osteoblasts to move and

attach to the eroded surface. This release of BDFs could either be due to matrix

metalloproteinase activity[15] or small osteoclasts that remain on the surface[16], though the

source is not modeled explicitly.

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Osteoclast resorption

We assume that each osteoclast resorbs bone in the direction with the maximum amount

of bone. Osteoclasts resorb bone tissue in areas where there is a high degree of

mechanical stress or strain. There are several proposed mechanisms governing how

osteoclasts detect areas of bone resorption. Integrins may play a role in guiding the

direction of bone resorption by regulating the formation and orientation of the sealing

zone. Specifically, integrins on the leading edge of the osteoclast are thought to sense

the mechanical properties of the bone tissue and orient the osteoclast towards areas of

higher mechanical stress or strain[17]. This results in the formation of a sealing zone that is

oriented in the direction of the mechanical stress or strain, allowing the osteoclast to

efficiently remove bone tissue from areas that are under the greatest mechanical load.

Another hypothesis is that osteoclasts may be guided by the orientation of collagen fibers

in bone[18]. Collagen is the main structural protein in bone, and it forms a network of fibers

that give bone its strength and resilience. Studies have suggested that osteoclasts may

be able to sense the orientation of collagen fibers in bone through a range of receptors

and signaling pathways, and that this information may guide their resorption activity.

Another hypothesis is that osteoclasts may be guided by chemical gradients of signaling

molecules that are produced by other cells in the bone microenvironment[17]. By following

these chemical gradients, osteoclasts may be able to target areas of bone where

remodeling is needed.

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To determine the direction, we check the Von Neumann neighborhood around each
subunit of the osteoclast and record the total amount of bone in each direction. If more
than one direction contains the maximum amount of bone, one of these directions is
randomly selected. The bone is removed from the grid as it is resorbed and is replaced
by the osteoclast. As bone is resorbed, bone derived factors are released from the bone
matrix[16], which is modeled as a production term in **Equation 10**. Because the amount of
bone that osteoclasts resorb is proportional to their lifespan, we verify that the average
amount of bone resorbed per osteoclast per year remains constant over time
(**Supplementary Fig. 1g**).

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1285   **Mesenchymal stem cells (MSCs)**

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Recruitment

MSCs have been identified in various niches within the bone marrow, and their precise
location and distribution are still under investigation. Some of the most common locations
where MSCs are found in the bone marrow are the endosteal region, the perivascular
region, and the central marrow region[19,20]) MSCs are located in close proximity to the
endosteal surface, where bone remodeling takes place, and the majority of MSCs are in
contact with blood vessels or surrounded by pericytes and other undefined cells, which
suggests that these cells are located in the perivascular niche[19,21]. After an osteoclast
fuses, an MSC is placed on the grid within a certain radius of the osteoclast (MSC_radius),
provided there is not already an MSC within the neighborhood. This requirement ensures
that MSCs are located adjacent to sites of bone remodeling to couple bone resorption
with bone formation[22]. However, to preserve that approximately 0.01% of the bone
marrow consists of MSCs[5], MSCs that are not within a certain radius of an osteoclast are
removed from the grid. Therefore, the number of MSCs fluctuates over time but is capable
of returning to the initial condition.

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1303   *Proliferation*

1304 We assume that MSCs divide only when BDF is above a certain threshold (BDF_{thresh})

1305 (**Supplementary Fig. 2c**). The probability of cell division is

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1307 $$p_{div} = 1 - \left(1 - f_{div}(BDF)\right)^{TIMESTEP\_AGENT} \#\#(4)$$

1308

1309 where

1310 $$f_{div}(BDF) = \{ \; 0 \qquad\qquad if\ BDF < BDF_{thresh} \quad \frac{\rho_{MSC}}{1 + \left(\frac{K_{MSC}}{BDF}\right)^2} \quad if\ BDF \geq BDF_{thresh} \; \#$$

1311 When an MSC divides we assume it undergoes asymmetric division, producing a

1312 precursor osteoblast. The daughter cell is randomly placed in an empty grid cell within

1313 the Moore neighborhood of the MSC.

1314

1315 *Movement*

1316 MSCs migrate in the direction of higher TGF-β when there is a cytokine gradient,

1317 otherwise they move randomly[16]. As before, we use the hybrid discrete-continuum

1318 technique to describe the probability of cell movement (**Equation 9**).

1319

1320 **Preosteoblasts**

1321

1322 *Death*

1323 We assume that preosteoblasts die if they are not adjacent to eroded bone with probability

1324

1325 $$p_{death} = 1 - (1 - pOB\_DEATH)^{TIMESTEP\_AGENT} \quad \#(5)$$

1326

1327 or with probability one if $pOB_{age} \geq 42\ days$. Once a preosteoblast dies it is immediately

1328 removed from the grid.

1329

Proliferation

We assume that high levels of BDF promote proliferation of preosteoblasts whereas low

levels promote differentiation [23]. The probability of cell division is the same as it is for

MSCs (**Equation 4**; **Supplementary Fig. 2c**), except that a preosteoblast divides

symmetrically to produce another preosteoblast. As before, the daughter cell is randomly

placed in an empty grid cell within the Moore neighborhood of the preosteoblast. To

assess whether these model assumptions qualitatively capture the dynamics of

proliferation in response to different concentrations of BDF, we inhibit BDF production by

multiplying the production rate by scale factor π_{Ti} (**Equation 10**). As expected, the

average proportion of preosteoblast over time decreases as BDF decreases

(**Supplementary Fig. 2e**).

1341

1342

1343   *Differentiation*

1344   After the bone resorption phase, preosteoblasts attach to the eroded surface and

1345   differentiate due to differentiation signals provided by the exposed bone matrix[22]. In the

1346   model, preosteoblasts that are adjacent to eroded bone and exposed to low levels of bone

1347   derived factors for two weeks will differentiate into active osteoblasts (osteoblasts).

1348

1349   *Movement*

1350   We assume the precursor osteoblasts that are not attached to eroded bone, move in

1351   response to a gradient of bone derived factors, which is modeled in the same way as for

1352   MSCs with the hybrid discrete-continuum technique (**Equation 9**).

1353

1354   **Osteoblasts**

1355

Death

Active osteoblasts ultimately either undergo apoptosis, become osteocytes, or become

quiescent bone-lining cells[9]. In the model, we assume that osteoblast death is

proportional to the amount of bone that was resorbed by the osteoclast subunit that had

occupied the space prior to the osteoblast (osteoclast_depth). Therefore, osteoblast

death is also proportional to the average time it takes for an osteoblast to form one unit

of bone (basal_time). This assumption permits the coupling of bone resorption with bone

formation, since the lifespan of an osteoblast controls how much bone the osteoblast

forms. Thus, bone homeostasis is maintained even when the amount of bone resorbed

by an osteoclast varies. Under normal conditions the lifespan of an osteoblast is

approximately 3 months[9], which we reproduce in our model (**Supplementary Fig. 1f**).

This equation describes how to define the lifespan of an aOB so that it lives long enough

to replace the bone resorbed by an aOC (during homeostasis).

1369

1370 $$aOB\_DEATH = basal\_time \cdot aOC\_depth \#(6)$$

1371   Units for equation 6:

1372   ○ aOB_Death: days

1373   ○ basal_time: days per unit of bone

1374   ○ aOC_depth: units of bone

1375

Alternatively, an active osteoblast may unintentionally get buried in bone by itself or other

osteoblasts during bone formation. This is comparable to an osteoblast becoming an

osteocyte, one of its potential cell fates. In the model, this occurs if the Von Neumann

neighborhood of an osteoblast only contains bone or other osteoblasts. When an

osteoblast is buried, this has possible consequences for bone homeostasis since the

osteoblast did not form as much bone as it would have had it completed its full lifespan.

To maintain a steady state of bone, the lifespan of the nearest osteoblast is increased to

allow it to build more bone to compensate for the amount lost due to the buried osteoblast.

This is a simplifying assumption of the model since biologically there are many factors

involved to regulate the number and lifespan of osteoblasts. However, several studies

have demonstrated the ability of osteoblasts, osteocytes and other cells of the BMU to

sense and communicate with one another through juxtacrine and paracrine signaling to

maintain bone homeostasis, through regulate cell proliferation, lifespan and activity [24-27].

1389

Bone Formation

We assume that the time it takes for an osteoblast to form a unit of bone is dependent on

the local concentration of BDF. To determine the functional relationship between BDF

and mineralization rate we use *in vitro* data from MC3T3-E1 cells cultured in osteoblastic

media with various concentrations of TGF-β or the TGF-β inhibitor, 1D11

(**Supplementary Methods 2.4**). This data shows how the mineralization rate compares

to the control, specifically that it increases as TGF-β decreases (**Supplementary Fig.**
2a). We approximate this trend using an exponential decay function and extract the
parameters using nonlinear least squares regression (**Supplementary Fig. 2b**):

$$f_{BF}(BDF) = (f_0 - Plateau) \cdot e^{-\delta_{BF} \cdot BDF} + Plateau \#(7)$$

This equation is unitless since it represents fold change to bone mineralization time.

1401

To determine the time that it takes an osteoblast to form one unit of bone as a function of
BDF, we scale the time it takes an osteoblast to form one unit of bone in basal levels of
BDF (basal_time) by **Equation 7**:

$$Mineralization\_Time(BDF) = \frac{basal\_time}{f_{BF}(BDF)} \#(8)$$

Units for equation 8:
○ Mineralization_Time: days per unit of bone
○ basal_time: days per unit of bone

1409

This scaling allows for mineralization to increase when BDF is below the basal level. In
the model, the mineralization time for each osteoblast is updated after sufficient time has
passed to form a unit of bone. To determine which direction to form bone, we impose a
set of rules to try to prevent the osteoblast from becoming buried and to prevent the
creation of large gaps in the placement of the bone. To do this, we first check the Von
Neumann neighborhood of an osteoblast for empty space. If more than one empty space
exists, the osteoblast will preferentially move to the location where it will remain in contact
with at least two units of bone and is not adjacent to another osteoblast; if this is not
possible, one of the empty spaces will be randomly selected. To form bone, the osteoblast
moves to the empty grid cell and its previous location is replaced with a new unit of bone.
Because the amount of bone that osteoblasts produce is proportional to their lifespan, we
verify that the average amount of bone produced per osteoblast per year remains
constant over time (**Supplementary Fig. 1h**). To assess whether these model
assumptions qualitatively capture the dynamics of mineralization in response to different
concentrations of BDF, we inhibit BDF production by multiplying the production rate by
scale factor π_{Ti} (**Equation 10**). As expected, BDF has a biphasic effect on bone in which

low BDF results in bone loss due to lack of MSC/preosteoblast proliferation and medium

BDF results in bone growth due to increased mineralization (**Supplementary Fig. 2d**).

1428

1429 **Movement**

1430

In the model, MSCs, preosteoblasts, and MM cells migrate in the direction of higher TGF-

β when there is a cytokine gradient, otherwise they move randomly[22]. preosteoclasts

migrate in response to a gradient of RANKL[12,13]. We use the technique for motility

described in the original implementation of the hybrid discrete-continuum model[14] to

describe the probability of each cell being stationary (P_0), moving left (P_1), right (P_2), down

(P_3), or up (P_4):

1437

1438
$$P_0 = 1 - \frac{4kD_n}{h^2} - \frac{k\chi}{h^2}\left(m_{i+1,j} + m_{i-1,j} + m_{i,j+1} + m_{i,j-1} - 4m_{i,j}\right) P_1$$

1439
$$= \frac{kD_n}{h^2} - \frac{k\chi}{4h^2}\left(m_{i+1,j} - m_{i-1,j}\right) P_2 = \frac{kD_n}{h^2} + \frac{k\chi}{4h^2}\left(m_{i+1,j} - m_{i-1,j}\right) P_3$$

1440
$$= \frac{kD_n}{h^2} - \frac{k\chi}{4h^2}\left(m_{i,j+1} - m_{i,j-1}\right) P_4$$

1441
$$= \underbrace{\frac{kD_n}{h^2}}_{Diffusion\,Term} + \underbrace{\frac{k\chi}{4h^2}\left(m_{i,j+1} - m_{i,j-1}\right)}_{Chemotaxis\,Term} \quad \#(9)$$

1442

1443 where the subscripts specify the location on the grid, i.e., $x = ih, y = jh$ where $\{i, j\}$ are

1444 positive integers, k denotes the timestep, $k = \Delta t$, and h denotes the spatial step, $h =$

1445 $\Delta x = \Delta y$. In the absence of a gradient of chemokine m, where $m = \{R_L, T_\beta\}$, cell

1446 movement is random with diffusion coefficient D_n, whereas in the presence of a gradient

1447 cell movement is directed with chemotaxis coefficient χ.

1448

1449 **Cytokines (RANKL and BDF)**

1450

1451 Receptor activator of NF-κB ligand (RANKL; R_L) is a cytokine that is produced in both

1452 soluble and membrane-bound forms and can activate osteoclasts. Recently, osteocytes

1453 have been identified as a major source of RANKL[28,29]. Once a microfracture occurs,

1454   RANKL is produced at the rate α_R at five adjacent cells on the perimeter of bone, which

1455   then diffuses in two spatial dimensions and degrades at the rate δ_R.

1456

Bone derived factors (BDFs; T_β) consist of the group of cytokines that are released during

bone remodeling, including TGF-β and IGF. These cytokines are produced in a latent

form by many other cell types, including T-cells, macrophages, and platelets[30]. Instead of

modeling the production of BDF explicitly by these other cell types, we assume that BDFs

are constantly produced at rate α_B, and further produced at rate α_T while bone is resorbed

by osteoclasts. We assume that BDF also diffuses in two spatial dimensions and

degrades at rate δ_T.

1464

1465
$$\frac{\partial R_L(x,y,t)}{\partial t} = D_R \underbrace{\left(\frac{\partial^2 R_L}{\partial x^2} + \frac{\partial^2 R_L}{\partial y^2}\right)}_{Diffusion} + \underbrace{\pi_{Ri}\alpha_R B_{i,j}}_{Production}$$

1466
$$- \underbrace{\delta_R R_L}_{Decay} \qquad \frac{\partial T_\beta(x,y,t)}{\partial t}$$

1467
$$= D_T \underbrace{\left(\frac{\partial^2 T_\beta}{\partial x^2} + \frac{\partial^2 T_\beta}{\partial y^2}\right)}_{Diffusion} + \underbrace{\pi_{Ti}\alpha_B}_{Basal\ Production}$$

1468
$$+ \underbrace{\pi_{Ti}\alpha_T B_{i,j} C_{i,j}}_{Production} - \underbrace{\delta_T T_\beta}_{Decay} \quad \#(10)$$

1469   where

1470 $\Omega_{i,j} = \{1 \quad if\ \Omega\ at\ (x_i, y_j)\ \ 0 \qquad otherwise \quad \Omega = bone\ cell\ (B)\ or\ osteoclast\ (C)$

1471

1472   *Boundary conditions of PDE grid*

1473   The system of PDEs is solved using the forward time centered space (FTCS) scheme

1474   with periodic boundary conditions imposed on all sides of the domain, which is

1475   implemented using the diffusion function in HAL. The timestep is chosen to ensure

1476   numerical stability, i.e., $\frac{D\Delta t_{diff}}{(\Delta x)^2} < \frac{1}{4}$.

1477

1478   **1.2. Incorporating Multiple Myeloma**

1479

1480   **Preosteoclasts**

1481

Fusion

Multiple myeloma cells enhance RANKL expression in the bone microenvironment which

leads to increased osteoclastogenesis[31]. In the model, we assume that if there are three

or more myeloma cells within the Moore neighborhood of a bone cell located on the

perimeter of bone, a new bone remodeling event is initiated. As described above, each

bone remodeling event is characterized by RANKL expression from five adjacent cells on

the perimeter of bone.

1489

1490 **Mesenchymal stem cells (MSCs)**

1491

1492 *Recruitment*

1493 Multiple myeloma cells produce chemoattractants that recruit MSCs to the bone

1494 marrow[32]. We assume that one MSC is recruited per 50 myeloma cells, and that once it

1495 is recruited, an MSC remains in the bone marrow (data not shown).

1496

Proliferation

Myeloma cells inhibit the differentiation of mesenchymal stromal cells through soluble

factors and cell-cell contract[33]. In the model, we assume that the differentiation of MSCs

to precursor osteoblasts occurs through asymmetric division. To capture the effect of

myeloma cells on osteoblast differentiation, we assume that MSCs do not divide if they

are within a certain radius of a myeloma cell (MM_radius).

1503

1504 **Preosteoblasts**

1505

1506 *Differentiation*

1507 Myeloma cells inhibit the differentiation of osteoblast progenitors through soluble factors

1508 and cell-cell contract[22]. In the model, we assume that preosteoblasts do not differentiate

1509 if they are within a certain radius of a myeloma cell (MM_radius),

1510

1511 **Multiple Myeloma**

1512

1513 *Initiation*

1514 A single myeloma cell is recruited within a certain radius of an osteoclast after the first

1515 osteoclast fusion event occurs.

1516

Death

The bone marrow microenvironment supports the growth and survival of multiple

myeloma cells[34]. To determine where myeloma cell death and division occur spatially in

the microenvironment, we measured the distance of these cells to the nearest bone

(**Supplementary Methods 2.8**; **Fig. 3a-d**). Because there is less cell death close to bone,

we assume that multiple myeloma cell death (sensitive and resistant cells) is dependent

on the local concentration of BDF. The probability of cell death is

1524

$$p_{death} = 1 - (1 - MM_{DEATH})^{TIMESTEP\_AGENT} \#(11)$$

where

$$MM_{DEATH} = \{ \ MM\_DEATH \qquad if \ BDF < BDF_{thresh} \ \ MM\_DEATH\_BDF \quad if \ BDF$$

$$\geq BDF_{thresh} \ \#$$

Proliferation

We assume that myeloma cell division is dependent on the concentration of BDF and has

maximum rate ρ_X. This maximum rate is dependent on if the myeloma cell is sensitive or

resistant, since we showed that the U266 cell line has a cost of resistance

(**Supplementary Fig. 7a-b**). Furthermore, we and others have shown that myeloma cell

division increases near MSC/preosteoblast[35] (**Fig. 3f** and **Fig. 6a**). To incorporate this

into the model, we assume that sensitive cells within a certain radius of an MSC or

preosteoblast divide faster than sensitive cells that are not close to an MSC or

preosteoblast (**Fig. 3g**), which divide faster than resistant cells. We define the probability

of cell division with the following Hill function:

1539

$$f_{div}(BDF) = \frac{\rho_X}{1 + \left(\frac{K_X}{BDF}\right)^2} \#(12)$$

where $\rho_X = \{MAX\_MM\_DIV, MAX\_MM\_DIV\_MSC, MAX\_R\_MM\_DIV\}$ and

$K_X = \{K_{MM}, K_{MM\_MSC}, K_{R\_MM}\}$ depending on if the myeloma cell is sensitive, resistant,

and/or within a certain radius of an MSC or preosteoblast (protect_radius). A Hill function

is chosen as the functional form because it is commonly used to represent cell responses

that are dependent on receptor-ligand interactions[11].

1546

1547

1548 **1.3. Incorporating Bortezomib**

1549

1550 **Preosteoclasts**

1551

1552 *Fusion*

1553 Bortezomib inhibits osteoclast differentiation *in vitro* in a dose-dependent manner[25]. To

1554 incorporate this into the model we multiply the probability of fusion (**Equation 2**) by a

1555 repressive Hill function so that the probability decreases as dose increases

1556 (**Supplementary Fig. 3d**):

1557

1558
$$f_{fusion\_BTZ}(RANKL, Dose) = f_{fusion}(RANKL) \cdot \frac{1}{1 + \left(\frac{Dose}{K_{dose}}\right)^2} \#(13)$$

1559 As expected, the total number of osteoclasts decreases as dose increases

1560 (**Supplementary Fig. 3g**).

1561

1562 **Osteoblasts**

1563

1564 *Bone Formation*

1565 Bortezomib enhances the mineralization rate of osteoblasts *in vitro* in a dose-dependent

1566 manner (**Supplementary Fig. 3b**). To incorporate this into the model we scale the

1567 mineralization time (**Equation 8**) linearly so that at maximum dose (Dose = 1) the time it

1568 takes an osteoblast to form a unit of bone is reduced by half (**Supplementary Fig. 3c**):

1569
$$Mineralization\_Time\_BTZ(BDF, Dose) = \frac{Mineralization\_Time(BDF)}{Dose + 1} \#(14)$$

1570

1571 As expected, the BA/TA increases as dose increases (**Supplementary Fig. 3f**) due to
1572 increased production of bone per osteoblast.

1573

1574 **Multiple Myeloma**

1575

Death

We assume that Bortezomib treatment does not affect the probability of cell death for
resistant cells. On the other hand, Bortezomib decreases viability for sensitive cells _in_
vitro and slows growth _in vivo_ in a dose-dependent manner (**Supplementary Fig. 3a** and
Fig. 6c)[36]._In vivo_, failure to eradicate the disease may be due to both cell intrinsic
mechanisms such as mutations, alterations in signaling pathways, copy-number
alterations, epigenetic changes, and cell extrinsic mechanisms such as environment
mediated drug resistance (EMDR)[37]. EMDR is when myeloma cells are transiently
protected from Bortezomib due to factors or interactions with other cells in the bone
microenvironment, which we define in our model to be when bone derived factors are
above a certain threshold or MSCs or preosteoblasts are within a certain radius of a
myeloma cell[32]. The probability of cell death during Bortezomib treatment is
(**Supplementary Fig. 3i**):

1589

1590
$$p_{death} = 1 - (1 - MM_{DEATH})^{TIMESTEP\_AGENT} \#(15)$$

where

$MM_{DEATH} = \{$ MM_DEATH $\quad$ $if\ RESISTANT\ and\ BDF$
$< BDF_{thresh}$ MM_DEATH_BDF $\quad$ $if\ RESISTANT\ and\ BDF$
$\geq BDF_{thresh}$ $MM\_DEATH(1 + 1.5 \cdot Dose)$ $\quad if\ SENSITIVE\ and\ BDF$
$< BDF_{thresh}\ and\ no\ MSC$
$/pOB$ MM_EMDR_DEATH $\quad if\ SENSITIVE\ and\ BDF$
$\geq BDF_{thresh}\ or\ MSC/pOB\ \#$

1598

1599 Therefore, tumor response to Bortezomib treatment depends on dose as well as the
1600 presence of bone derived factors or MSCs/preosteoblasts. At high dose, it is possible to

1601 completely eradicate the tumor in the absence of EMDR, similar to what is observed in *in*

1602 *vitro* experiments (**Supplementary Fig. 3j**).

1603

1604 *Proliferation*

1605 Once treatment is initiated, myeloma cells have a probability of developing resistance (p_Ω)

1606 during cell division that would cause the cell to become resistant to bortezomib.

1607

1608 **Dose selection**

1609

1610 *Bortezomib*

1611 We define dose to be between 0 and 1, where 0 represents no treatment and 1 represents

1612 the maximum dose, i.e., the dose that is sufficient to kill off sensitive cells without having

1613 a major impact on normal bone cells such as MSCs and preosteoblasts. Based on the *in*

1614 *vitro* cell viability assay, we define maximum dose to be 10 nM (**Supplementary Fig. 3a**).

1615

1.4. Parameter Exploration

Parameter estimates used in the HCA model may vary widely based on the experimental

design. For example, MM cell proliferation and death rates vary depending on the MM

cell line used, growth media, and/or cell-cell interactions. To test whether our results are

dependent on a particular parameter value, select parameters were varied to assess how

the relapse time (when MM burden reached 20% of the marrow) and proportion of

sensitive cells at endpoint changed under continuous bortezomib treatment

(**Supplementary Fig. 10**). We found that the parameter controlling the impact of EMDR

had a more striking effect on the proportion of sensitive cells at endpoint instead of the

relapse time (**Supplementary Fig. 10b**), whereas the parameter controlling the cost of

resistance had an impact on both outputs in the presence of EMDR (**Supplementary Fig.**

10c). Furthermore, the parameter controlling the survival advantage of BDF under no BTZ

treatment conditions had only a minor impact on either output (**Supplementary Fig. 10d**),

whereas the parameter controlling the proliferative advantage of sensitive cells in the

presence of MSC/preosteoblast had a strong effect on the proportion of sensitive cells at

endpoint. However, when the proliferative advantage is sufficiently strong, minimal

residual disease may be present in the presence or absence of EMDR, though the
proportion is higher with EMDR (**Supplementary Fig. 10e**). This analysis shows that
although the proportion of sensitive cells at endpoint varied, our finding that EMDR
maintains a reservoir of sensitive cells was robust for these parameters. Furthermore, we
showed that EMDR consistently led to a higher proportion of tumors that relapsed, except
when the proliferative advantage due to MSC/preosteoblast was sufficiently large.

1638

1639 **1.5. Parameters**

1640

The HCA model contains a large number of parameters as it has six different cell types
and two microenvironmental factors. Many of the parameters were difficult to obtain and
had to be estimated. Because many of the cell actions, such as proliferation and
chemotaxis, result from the combination of parameters rather than a single value, our
goal is to capture key outputs such as bone remodeling homeostasis instead of precisely
parameterizing the model.

1647

1648 **Supplementary Table 1: Grid Parameters**

Grid Parameter	Description	Value	Units	Source
SPACESTEP (Δx)	Space step of HCA grid	10.0	μm	Estimated*
TIMESTEP_AGENT (Δt_{cells})	Cell timestep	0.1	*hour*	Assumed
N_TIMESTEP_PDE	Number of diffusion timesteps per agent timestep	360	number	Assumed
TURNOVER_TIME	Turnover time of trabecular bone	35040	*hours*	[9]
xDim	Length of HCA grid	1600	μm	Assumed
yDim	Height of HCA grid	1500	μm	Assumed

1649 ● *SPACESTEP*. We assume that $1\ pixel\ =\ 10\ \mu m$, the diameter of a myeloma cell (experimentally
1650 derived)

1651

1652 **Supplementary Table 2: BDF/RANKL Parameters**

BDF/RANKL Parameter	Description	Value	Units	Source

---	TGF-β in bone	0.2	ng/mg	[38]
$TGFB\_DiffCoef$ (D_T)	BDF diffusion coefficient	780	$\mu m^2/min$	[39-42]
$RANKL\_DiffCoef$ (D_R)	RANKL diffusion coefficient	780	$\mu m^2/min$	Assumed
$TGFB\_productionRate$ (α_T)	BDF production rate	2.04×10^{-9}	$(ng/\mu m^3) \cdot cell_{unit}^{-1} \cdot min^{-1}$	Estimated*
$RANKL\_productionRate$ (α_R)	RANKL production rate	2.04×10^{-9}	$(ng/\mu m^3) \cdot cell_{unit}^{-1} \cdot min^{-1}$	Assumed $\alpha_R = \alpha_T$
$TGFB\_basalRate$ (α_B)	BDF basal production rate	2.04×10^{-11}	$(ng/\mu m^3) \cdot min^{-1}$	Estimated*
$TGFB\_decayRate$ (δ_T)	BDF decay rate	0.35	min^{-1}	[43]
$RANKL\_decayRate$ (δ_R)	RANKL decay rate	0.35	min^{-1}	Assumed $\delta_R = \delta_T$
$maxTGFB$ (BDF_{max})	Maximum BDF at given location	8.7×10^{-10}	$ng/\mu m^3$	Estimated
Ts (BDF_{basal})	Basal BDF	$\dfrac{\alpha_B}{\lvert \delta_T \rvert \cdot BDF_{max}}$	$unitless$	Estimated
$TGFBthresh$ (BDF_{thresh})	Threshold BDF	$1.05 \cdot BDF_{basal}$	$unitless$	Assumed
$maxRANKL$ $(RANKL_{max})$	Maximum RANKL at given location	1.7×10^{-9}	$ng/\mu m^3$	Estimated
$Extra\_TGFBtime$	Duration of BDF expression during reversal phase	72	$hours$	Assumed
max_RANKL_on	Maximum duration of RANKL	336	$hours$	Assumed

1653   ●   *TGF-β diffusion rate, D_T.* The $780 \ \mu m^2/min$ was estimated using the molecular weight of TGF-β

1654   (25 kDa [39]). A molecule of molecular weight (M) 0.3-0.5 kDa has a diffusion coefficient of

1655   approximately $10^{-6} \ cm^2/s$ [40]. The plot of $\log \log (D)$ vs. $\log \log (M)$ correlates with a line of

1656   slope $-\frac{1}{3}$ [41]. Thus, we solve

1657 $(D) = (10^{-6}) + \frac{1}{3}\big((0.5) - (25)\big)$

 to get $D = 2.6 \times 10^{-7}\ cm^2/s = 1560\ \mu m^2/min$. Small molecules diffuse through the extracellular

space with an effective diffusion coefficient that is two to three times less than the free diffusion

coefficient[42], thus $D^* = D/2 = 780\ \mu m^2/min$.

• *TGF-β production rate, α_B.*

○ Volume of resorption pit: $\pi r^2 h = \pi(25^2)(10) = 19634.95\ \mu m^3/day$, where r = radius of

osteoclast and h = amount of bone resorbed per day

○ Rate of bone resorption by a $50\ \mu m$ OC: Given the density of bone = $1500\ kg/m^3$ [44],

$(1500\ kg/m^3) \times (19634.95\ \mu m^3/day) \times (10^{-18}\ m^3/\mu m^3) = 2.945 \times 10^{-11}\ kg/day =$

$2.945 \times 10^{-5}\ mg/day$

○ TGF-β released/day due to bone resorption by a 50 μm OC: Given concentration of TGF-

β in bone is 0.5 ng/mg [38], $(2.945 \times 10^{-5}\ mg/day) \times (0.5\ ng/mg) = 1.47 \times 10^{-5}\ ng/$

day. Because a $50\ \mu m$ OC takes up 5 pixels, we divide this by 5 to get:

$2.94 \times 10^{-6}\ ng \cdot cell_{unit}^{-1} \cdot day^{-1} = 2.04 \times 10^{-9}\ ng \cdot cell_{unit}^{-1} \cdot min^{-1}$, consistent with [45].

We convert this to units of ng per volume to be consistent with the units of chemotaxis,

which requires dividing the amount (ng) by the soluble volume of each grid point. Because

the soluble volume fraction is unknown, we set $\alpha_T = 2.04 \times 10^{-9}\ (ng/\mu m^3) \cdot cell_{unit}^{-1} \cdot$

min^{-1}, which was calibrated to reproduce the steps of normal bone remodeling.

1675

• *TGF-β basal production rate, α_B.* We assume that BDF is produced at a higher rate through bone

resorption compared to other sources in HCA[22]

• *TGF-β decay rate, δ_T:* The half-life of *TGF-β* is 2 minutes[44]. Thus, the decay rate is $\frac{lnln\ (2)}{2} =$

$0.35\ min^{-1}$.

• maxTGFβ was determined by running the unnormalized model a number of times and

then recording the maximum TGFβ at a single grid point. This value of BDF was then set

as maxTGFβ. The maximum TGFβ is printed after each model is run (tmax) so that it can

be monitored whether the value stays between 0 and 1.

• Ts is the basal BDF and is defined as written in the table, $\alpha_B/(|\delta_T| \cdot BDF_{max})$ .This is the

amount of BDF that is always present on the grid.

• MaxRANKL was determined by running the unnormalized model a number of times and then

looking at the output "preosteoblastborn.csv" to evaluate the maximum value of RANKL that

occurred when an osteoclast formed. This value of RANKL was then set as maxRANKL so that

most values of RANKL that lead to the formation of an osteoclast are between 0 and 1 (however,

it is possible that some values in future runs of model are not strictly below 1).

1691

1692

1693

Supplementary Table 3: preosteoclast/osteoclast Parameters

preosteoclast/osteoclast Parameter	Description	Value	Units	Source
$pOC\_DiffCoef$	preosteoclast random motility	0.3	$\mu m^2/min$	Estimated
$pOC\_TaxisCoef$	preosteoclast chemotaxis coefficient	5×10^{10}	$\mu m^2 min^{-1}(ng/\mu m^3)^{-1}$	Estimated
K_{aOC}	Half-maximal concentration constant	0.01	$concentration$	Assumed
μ_{OC}	Mean osteoclast lifespan	14	$days$	[9,46]
σ_{OC}	osteoclast lifespan standard deviation	7/3	$days$	Assumed
OC_{min}	Minimum osteoclast lifespan	7	$days$	Assumed
OC_{max}	Maximum osteoclast lifespan	21	$days$	Assumed
MAX_FUSION_RATE	Maximum fusion rate	1/72	$hours^{-1}$	[47]
$Unit\_RESORPTION$	Time to resorb one unit of bone	1	day	[48]
$aOC\ diameter$	Diameter of osteoclast	50	μm	[10]

- *Random motility coefficient of cell, preosteoclast_DiffCoef*: Stokes-Einstein relation: $D = \frac{k_B T}{6\pi\eta a}$. Given $k_B = 1.38 \times 10^{-23}\ N \cdot m, T = 310\ K$ (body temp: $310\ K$; room temp: $300\ K$), $\eta = 10^{-3}\ N \cdot s/m^2$ (viscosity of water), $a = 5\ \mu m$ (cell radius), $D = 4.54 \times 10^{-10} cm^2 s^{-1} = 3\ \mu m^2/min$. We assume that preosteoclast random motility is 10-fold slower in bone marrow compared to water.

Supplementary Table 4: MSC/preosteoblast/osteoblast Parameters

MSC/preosteoblast/osteoblast Parameter	Description	Value	Units	Source
$MSC\_DiffCoef = pOB\_DiffCoef$	MSC/preosteoblast random motility	0.03	$\mu m^2/min$	Estimated

$MSC\_TaxisCoef$	MSC chemotaxis coefficient	5×10^9	$\mu m^2 min^{-1}(ng/\mu m^3)^{-1}$	Estimated
$pOB\_TaxisCoef$	preosteoblast chemotaxis coefficient	5×10^{11}	$\mu m^2 min^{-1}(ng/\mu m^3)^{-1}$	Estimated
$K_{MSC} = K_{pOB}$	Half-maximal concentration constant	$\sqrt{3} \cdot BDF_{thresh}$	$unitless$	Assumed
$MAX\_MSC\_DIVISION\_RATE = MAX\_pOB\_DIVISION\_RATE$ $(\rho_{MSC} = \rho_{pOB})$	Maximum proliferation rate	$1/24$	$hour^{-1}$	Assumed
pOB_DEATH	preosteoblast death rate	$1/72$	$hour^{-1}$	Assumed*
pOB_DIFF	preosteoblast differentiation time	336	$hour$	Determined from experiments
MSC_radius	Radius around osteoclast/MM to recruit MSC	40	μm	Assumed*
MM_radius	Radius of MM effect on MSC/preosteoblast differentiation	80	μm	Assumed*
$Y0$ (f_0)	Maximum fold change	5.055	$unitless$	Estimated*
$Plateau$	Minimum fold change	0.5379	$unitless$	Estimated*
$scalefactor$	Scale factor	$\dfrac{19.2}{BDF_{basal}}$	$unitless$	Estimated*
k (δ_{BF})	Fold change decay constant	$0.1136 \cdot scalefactor$	$unitless$	Estimated*

basal_time	Basal unit bone formation time	9	*days*		49

● *Random motility coefficient of cell, MSC_DiffCoef, preosteoblast_DiffCoef*: We assume that MSC
and preosteoblast random motility is 100-fold slower in bone marrow compared to water, and 10
fold slower than preosteoclast.

● *Chemotaxis coefficient, MSC_TaxisCoef, preosteoblast_TaxisCoef*: The chemotaxis coefficient of
human neutrophils in response to the tripeptide FNLLP is
$150 \, cm^2 s^{-1} M^{-1} \approx 5.18 \times 10^{-2} mm^2 (pg/mm^3)^{-1} day^{-1} = 3.6 \times 10^{13} \mu m^2 (ng/\mu m^3)^{-1} min^{-1}$
(using 25 kDa as the molecular weight of TGF-β)[50,51]. However, to give reasonable model outputs
required us to calibrate this parameter further and assume that MSC_TaxisCoef <
preosteoblast_TaxisCoef.

● *preosteoblast death rate, preosteoblast_DEATH*: Assumed to be same as preosteoclast[47]

● *MSC recruitment radius, MSC_radius*: Defined so that MSC is close enough to respond to BDF
generated by osteoclast

● *MM radius of impact on MSC/preosteoblast, MM_radius*: Defined so that MSC/preosteoblast
responds to MM even when not directly adjacent. This assumption was necessary since HCA
assumes MM is unable to migrate towards MSC/preosteoblast in absence of BDF, which created
distance between MM and MSC/preosteoblast.

● *Exponential decay* (**Equation 7**)*: Y0, Plateau, k*: These values were estimated by using an
exponential decay function and nonlinear least squares regression with *in vitro* data from MC3T3-
E1 cells cultured in osteoblastic media with various concentrations of TGF-β or the TGF-β inhibitor,
1D11 (**Supplementary Methods 2.4**).

1721

1722 **Supplementary Table 5: MM Parameters**

MM Parameter	Description	Value	Units	Source
MM_DiffCoef	MM random motility	0	$\mu m^2/min$	Assumed
MM_TaxisCoef	MM chemotaxis coefficient	5×10^9	$\mu m^2 min^{-1} (ng/\mu m^3)^{-1}$	Estimated
MM_DEATH	MM basal death rate	1/120	$hour^{-1}$	Assumed*

MM_EMDR_DEATH	MM death rate with EMDR	1/120	$hour^{-1}$	Assumed*
MM_DEATH_BDF	MM death rate with BDF	1/1200	$hour^{-1}$	Assumed*
MAX_MM_DIVISION_RATE	Maximum proliferation rate	1/24	$hour^{-1}$	Estimated
MAX_MM_DIV_MSC	Maximum proliferation rate	1/24	$hour^{-1}$	Assumed
MAX_RESISTANT_DIVISION_RATE	Maximum proliferation rate	1/48	$hour^{-1}$	Estimated
K_{MM}	Half-maximal concentration constant	$\sqrt{3} \cdot BDF_{thresh}$	$unitless$	*
K_{MM_MSC}	Half-maximal concentration constant	BDF_{basal}	$unitless$	*
K_{R_MM}	Half-maximal concentration constant	$\sqrt{1.25} \cdot BDF_{basal}$	$unitless$	*
protect_radius	Radius of MM birth/death advantage from MSC/preosteoblast	20	μm	Assumed
$p\,resistance(p_{\Omega})$	Resistance probability	$variable$	unitless	Assumed

●   *Random motility coefficient of cell, MM_DiffCoef*: We assume that MM cells do not have random
motility.

●   *Chemotaxis coefficient, MM_TaxisCoef*: We assume that MM_TaxisCoef = MSC_TaxisCoef.

●   *MM death rates, MM_DEATH, MM_EMDR_DEATH, MM_DEATH_BDF*: We assume that the
lifespan of MM is similar to short-lived (3-5 days) and long-lived (several months) plasma cells[52]

● *Half maximal constant, K_{MM}.* We set $K_{MM} = \sqrt{3} \cdot BDF_{thresh}$, the value of BDF for which the myeloma

proliferation rate is half maximum. This is estimated under the assumption that when $BDF =$

BDF_{thresh}, i.e., when BDF is slightly above the basal level that is constantly present, the

proliferation rate = 1/96 hour^{-1}. This value is based on the doubling time of myeloma cells *in vivo*.

● *Half maximal constant, K_{MM_MSC}.* We set $K_{MM\_MSC} = BDF_{basal}$, which is estimated under the

assumption that when $BDF = BDF_{basal}$, i.e. in locations in the bone marrow that are not close to

bone resorption, the myeloma proliferation rate = 1/48 hour^{-1} in the presence of MSC/preosteoblast

(i.e. half the maximum proliferation rate).

● *Half maximal constant, K_{R_MM}.* We set $K_{R\_MM} = \sqrt{1.25} \cdot BDF_{basal}$, which is estimated so that when

$BDF = BDF_{basal}$, the division rate of resistant myeloma cells is less than the division rate of

sensitive myeloma cells and remains greater than the death rate in the absence of Bortezomib

treatment.

1740

1741 **Supplementary Table 6: BTZ Parameters**

BTZ Parameter	Description	Value	Units	Source
K_{dose}	Half-maximal concentration constant	0.05	*unitless*	Assumed

1742

1743 **2. Biological Supplementary Methods**

1744

2.1. Cell culture

Human proteasome inhibitor sensitive (U266) myeloma cell and their proteasome inhibitor

resistant derivatives (PSR[53,54]) were a kind gift from Dr. Steven Grant at the University of

Virginia, VA. U266 and PSR were transduced using QIAGEN lentiviral particles (CLS-

PCG-8 or CLS-PCR-8) according to manufacturer's instructions to express GFP and RFP

respectively, generating U266-GFP and PSR-RFP. These cells were cultured in RPMI

containing 10% FBS (PEAK), 1% penicillin-streptomycin. MCSF-generated macrophages

were isolated as previously described[55,56]. Briefly, tibia and femur were harvested from 6-

week-old C57Bl/6 RAG2-/- mice. Bone marrow cells were collected by centrifugation

(10,000 g, 15s) cells were plated aMEM (+/+) containing 10% FBS (Peak), 1% penicillin-

streptomycin and MCSF (300-25, Peprotech; 30ng/ml). Adherent macrophages were

collected and used for downstream experiments after 72 hours. Murine mesenchymal

stromal cells (MSCs) were isolated as previously described[57]. Human MSCs (PT-2501) and the murine preosteoblast cell line, MC3T3-E1 were purchased from Lonza and ATCC, respectively. Mouse MSCs and MC3T3-E1 cells were cultured in aMEM (-/-) containing 1% penicillin-streptomycin and 15 or 10% FBS (PEAK), respectively. Human MSCs were cultured as above except with 10% qualified FBS (Gibco).

2.2. MTT Assay

Myeloma cell lines, mouse MSCs or MC3T3-E1 were plated in 96-well plates at a density of 1×10^4 cells/well. Cells were treated with vehicle or a range of concentrations of zoledronate or bortezomib. Cell viability was assessed at 72 hours by the MTT assay following the manufacturer's instructions (CellTiter 96, #G3582, Pierce.) The absorbance was measured at 490nm after 3 hours of incubation at 37°C.

2.3. Osteoclastogenesis Assay

Osteoclast formation assays were performed using murine MCSF-generated macrophages as previously described[55,56]. Briefly, MCSF-generated macrophages from 4–6-week-old C57Bl/6 RAG2-/- mice were plated in a 96-well plate (25×10^3 cells/well) in triplicate with MCSF (30ng/ml) and allowed to adhere for 24 hours. RANKL (315-11C, Peprotech) was given at the indicated doses with M-CSF on days 1 and 3. Cultures were fixed with 4% paraformaldehyde on day 5 and TRAcP stained. TRAcP positive multinucleated (>3) were deemed osteoclasts.

2.4. Osteoblast mineralization assay

Mouse MSCs, MC3T3-E1 cells or human MSCs (huMSCs) were differentiated with 1X StemXVivo mouse/rat or human osteogenic supplement (CCM009; R&D Systems) for indicated number of days. To assess the effect increased TGF-β has on OB differentiation, either exogenous human TGF-β1 (240-B; R&D systems) or vehicle (PBS) was added to cultures. To assess the effect decreased TGF-β levels have on OB differentiation, either anti-TGF-β antibody (1D11; R&D systems) or isotype control (13C4; R&D systems) was added to cultures. OB mineralization was assessed by Alizarin red staining as previously described[55,56]. Conditioned medium was generated from huMSCs

1788 or huMSCs differentiated for 7-28 days in osteogenic supplement by incubating cells in
1789 standard aMEM for 24hours.

1790

2.5. MM-MSC and sensitive/resistant MM co-culture assays

Human MSCs (huMSCs; Lonza) were plated (2000 cells/100ul) or media alone in a 96

well plate and allowed to adhere overnight. The following day 50% of the media was

removed and replaced with media containing U266-GFP+ MM cells in standard RPMI.

Plates were centrifuged at 200g for 5 minutes to facilitate adhesion to MSCs. After 3

hours, bortezomib was added at indicated concentrations. Images were taken at 0 and

72 hours. The area covered by GFP+ MM cells was calculated in Fiji software[58]. U266-

GFP and PSR-RFP (10,000 total cells/well,) were plated at indicated ratios in a 96-well

plate with indicated concentrations of bortezomib. Cell confluency for GFP and RFP

populations was measured every 12 hours using Incucyte S3. For long term (60 day and

30 day cultures). Cultures were set up as previously described. BTZ (10nM) was given

over 72 hour periods and PI-sensitive U266 and PI-resistant PSR confluency was

measured by fluorescent markers using the incucyte SX5. After treatment, media was

replaced, after PBS washing, with standard RPMI. Images were taken at indicated

timepoints with EVOS FL auto prior to media changes.

1806

2.6. Flow cytometry

Left tibiae were used to assess tumor burden by GFP expression. Tibial ends were

excised, whole bone marrow was isolated by centrifugation at 10,000g for 10 seconds.

Red blood cells were lysed by RBC lysis buffer (R7757, Sigma-Aldrich) as per

manufacturers guidelines. Bone marrow cells were subject to viability staining with

Zombie Near-Infrared (NIR; 1:500; 423105, BioLegend). Appropriate compensation and

fluorescence-minus-one (FMO) controls were generated in parallel either with aliquots of

bone marrow cells or U266$^{GFP+/-}$. Stained controls and samples were analyzed using BD

Biosciences LSRII flow cytometer. The percentage of GFP-expressing cells was gated

on singlet live bone marrow cells in FCS Express 7. To address the proliferative

advantages provided by cells of the BME to MM cells, U266 MM cells were stained with

CM-DIL (Invitrogen; V22888) according to the manufacturer's instruction and incubated

with 50% (v/v) control, MSC, preosteoblasts (Day 7 or 14) or OB (day 21 or 28)

conditioned media for 7 days, with media changes every 3 days. An aliquot of untreated

CM-DIL+ cells was stained with Zombie NIR as above and used for baseline time point.

At the end of the experiment, MM cells were stained with Zombie NIR for live/dead

discrimination. The MFI for the CM-DiI channel was calculated at baseline and after 72

hours on live single cell cells using appropriate FMO controls. FCS Express 7 was used

to calculate the proliferative index of these cells.

1826

1827 2.7. Microcomputed Tomography

Harvested right tibiae were fixed in 4% paraformaldehyde for 48 hours. Tibiae from mice

from all time points were centralized and were subjected to micro-computed topography

(µCT) scanning using SCANCO µ35 scanner to elucidate bone volume data at the

proximal tibial metaphases. Individual bone scans were deidentified using numerical

codes during, and reidentified post analyses in a blinded fashion. Evaluation of trabecular

bone microarchitecture was performed in a region that consisting of 1000 µm, beginning

500µm from the growth plate. A three-dimensional cubical voxel model of bone was built,

and calculations were made for relative bone volume per total volume (BV/TV), trabecular

number (Tb.N), trabecular thickness (Tb.Th), trabecular spacing (Tb.Sp) and connectivity

density (Conn.D).

1838

1839 2.8. Immunofluorescence

Tibiae were decalcified in an excess of 10% EDTA for 21 days, refreshing EDTA every

48 hours before being placed in 30% sucrose (w/v) for 48 hours and subsequent

cryosectioning. Tibia were mounted on Superfrost Plus slides (Fisher) with optimal cutting

temperature (OCT) media and frozen on dry ice. Using a cryostat, 20 µm sections were

made and stored at -80°C. For immunofluorescence, sections were kept on a slide

warmer overnight at 56°C. Sections were rehydrated for 30 minutes at room temperature

in PBS. Sections were blocked with 10% (v/v) normal goat serum and washed in PBS

before staining addition of primary antibodies. Sections were incubated overnight at 4°C

with primary rabbit antibodies at a dilution of 1:100 (anti-pHH3; 06-570 Millipore, anti-

Osterix; ab22552, abcam: anti-aSMA: PA5-16697, Invitrogen,). Subsequently, slides

were washed thrice in PBS and stained with goat anti-rabbit Alexa Fluor-647-conjugated

secondary antibody (1:1000) at room temperature for 1h. DAPI (1ng/ml) was used as a

nuclear counterstain. Mounted sections were imaged using 10X image tile-scans of whole

tibia. The number of pHH3+ nuclei that co-localized with GFP+ cells were counted and

the distance to nearest bone (tibia or cortical) was calculated. For MSC analyses, the

percentage of total area in the trabecular region that was covered by αSMA+ cells were

calculated on Fiji software. For preosteoblasts, the number of Osterix+ nuclei were

counted and normalized to perimeter of trabecular bone for each mouse (Osx$^+$ cells/mm).

1858

2.9. Histomorphometry TRAcP and ALP analyses

Additional tibia bone sections were cryosectioned and baked at 42°C overnight to improve

tissue adhesion while retaining endogenous enzymatic activity. Tibial bone sections were

rehydrated in PBS before incubation in napthol-AS-MX phosphate (Sigma-Aldrich; 855-

20) and fast blue RR salt (Sigma-Aldrich; FB25-10CAP) solution for 30 minutes to identify

ALP+ regions with a dark blue stain. After washing in PBS, the same sections were

incubated in basic stock solution for 5 minutes at 37°C. Tibial sections were developed in

pararosaniline dye and sodium nitrite at 37°C for 3 minutes to highlight red TRAcP+ cells.

Sections were further counterstained with hematoxylin to visualize bone morphology.

Slides were mounted and imaged using EVOS Auto brightfield at 20X magnification. Five

images per section were taken and the number of ALP+ cuboidal bone-lining osteoblasts

and red multinucleated TRAcP+ osteoclasts per bone surface were calculated.

1871

2.10 Ex vivo mathematical myeloma advisor (EMMA) platform: Pentecost Myeloma

Research Center cohort. An *ex vivo* assay was used to quantify the chemosensitivity of primary

MM cells[59-61]. Fresh BM aspirate cells were enriched for CD138$^+$ expression using Miltenyi

(Bergisch Gladbach, Germany) 130-051-301 antibody-conjugated magnetic beads. MM cells

(CD138$^+$) were seeded in Corning (Corning, NY) CellBIND 384 well plates with collagen I and

previously established human-derived stroma, containing approximately 4000 MM cells and 1000

stromal cells. Each well was filled with 80 µL of Roswell Park Memorial Institute (RPMI) 1640

media supplemented with fetal bovine serum (FBS, heat inactivated), penicillin/streptomycin, and

patient-derived plasma (10%, freshly obtained from patient's own aspirate, filtered) and left

overnight for adhesion of stroma. The next day, drugs were added using a robotic plate handler

so that every drug/combination was tested at 5 (fixed concentration ratio, for combinations)

concentrations (1:3 serial dilution) in two replicates. Negative controls (supplemented growth

media with and without the vehicle control dimethyl sulfoxide [DMSO]) were included, as well as

positive controls for each drug (cell line MM1.S at highest drug concentration). Plates were placed

in a motorized stage microscope (EVOS Auto FL, Life Technologies, Carlsbad, CA) equipped with

an incubator and maintained at 5% CO_2 and 37 °C. Each well was imaged every 30 min for a total

duration of up to 6 days. A digital image analysis algorithm[59-61] was implemented to determine

changes in viability of each well longitudinally across the 96 or 144hr intervals. This algorithm

computes differences in sequential images and identifies live cells with continuous membrane

deformations resulting from their interaction with the surrounding extracellular matrix. These

interactions cease upon cell death. By applying this operation to all 288 images acquired for each

well, we quantified non-destructively, and without the need to separate the stroma and MM, the

effect of drugs as a function of concentration and exposure time. Digital image analysis computes

percent viability of MM cells for each time point and experimental condition (drug and

concentration). For each patient-drug, we have a dose-time-response surface, which is abstracted

into AUC (area under the curve), which is an area/integral measure of *ex vivo* response to therapy

computed by taking an average of all *ex vivo* responses across all time (first 96h) and

concentration. Clinical data was matched to patient samples ex vivo. Samples in the lowest AUC

quartile were considered sensitive.

1901

1902

1903

1904   **2.10. Statistical Analysis**

1905   Statistical analysis was performed using the analysis of variance (ANOVA) with the

1906   appropriate post multiple comparison analysis in GraphPad prism 8.0-10.0.

1907

1908　**Supplementary Figures and Legends**

1909

Supplementary Fig. 1. HCA captures key features of normal bone remodeling.

1913   **a.**   Interaction diagram (left) between cell types in the HCA and factors such as BDFs

1914   and RANKL (created with biorender.com). Table of references and experimental

1915   systems in which results were obtained (right).

1916   **b.**   HCA flow diagram adapted from Bravo et al. (2020)[6].

1917   **c.**   HCA model outputs of bone area to total area (BA/TA)

1918   **d.**   HCA model outputs of MSC content.

1919   **e.**   HCA model outputs of osteoclast numbers, and osteoblast numbers.

1920   **f-g**, Mean lifespan of osteoclasts **(f)** and osteoblasts **(g)** over 4 years of normal bone

1921   homeostasis. **h,** Mean units of bone resorbed per osteoclast each year of simulation.

1922   **i,** mean units of bone produced per osteoblast over course of the 4-year simulation.

1923

1925

Supplementary Fig. 2. Inhibition of bone microenvironment cytokines in the HCA.
a, The preosteoblast cell line MC3T3-E1 was cultured in osteogenic supplement with indicated concentrations of either isotype control antibody 13C4 or anti-TGF-β neutralizing antibody 1D11 (left) or TGF-β1 (right) for 14 days. Alizarin red was used to identify mineralized area. Results are normalized to isotype/vehicle-treated controls. Representative images of alizarin staining from control and highest

1932 concentrations (below). **b-c**, Plots of functional forms used to represent the fold change

1933 to osteoblast mineralization rate (**b**) and MSC/preosteoblast division rate (**c**). The black

1934 dots (**b**) represent the data from the *in vitro* experiments with the MC3T3-E1 cells that

1935 were used to fit the exponential decay function, as described in section 1.1 of

1936 supplementary methods. The red dot (**c**) represents the lack of MSC/preosteoblast

1937 division rate when BDF is at a basal level (dotted red line), and the black dot (**c**)

1938 represents the division rate when BDF is at the threshold level for proliferation (dotted

1939 black line). Another black dot highlights the half maximum division rate defined by the Hill

1940 function.

1941 * $p < 0.05$ ** $p < 0.01$, *** $p < 0.001$, **** $p < 0.0001$.

1942

1943

Supplementary Fig. 3. The impact of bortezomib (BTZ) on cells of the myeloma bone microenvironment *in vitro* and *in silico*. a, Sensitive U266 (S-MM) and resistant PSR (R-MM) myeloma, murine mesenchymal stromal cells (MSCs) and the preosteoblast cell line MC3T3-E1 (preosteoblast) were treated with varying

concentrations of BTZ. Viability was measured after 72 hours by MTT assay. Results are

normalized as percentage of control. **b**, the preosteoblast cell line MC3T3-E1 were

cultured in osteogenic supplement with indicated concentrations of BTZ. Alizarin red was

used to identify mineralized area. Results are normalized to vehicle-treated controls. **c-d**,

Plots of functional forms used to represent the osteoblast mineralization time (**c**) and

the probability of preosteoclast fusion (**d**) with indicated concentrations of bortezomib. **e**,

Interaction diagram of normal bone cells with bortezomib. Red line denotes inhibition,

black like indicates stimulation. **f-h**, Computational outputs of bone area to total area

ratio (**f**), cumulative number of osteoclasts (**g**), and units of bone resorbed per osteoclast

(**h**) following treatment of normal bone model with indicated concentrations of bortezomib.

Treatment begins on day 365 (black dotted line) and is applied continuously for 3 years. **i**,

Plot showing S-MM and R-MM death rate as a function of bortezomib with/without (+/-)

BDF and +/- EMDR. **j**, Model outputs of MM growth with high and low doses of bortezomib

with/without EMDR. Treatment begins when MM/MA=10% (black dotted line) and is

applied continuously until MM/MA=20%. **k**, Flow chart outlining decisions MM cells

make under BTZ treatment   *** p<0.001.

1964

Supplementary Fig. 4. The impact of zoledronate (ZOL) on cells of the myeloma bone microenvironment *in vitro* and in *silico*. a, Sensitive U266 (S-MM) and resistant PSR (R-MM) myeloma, murine mesenchymal stromal cells (MSCs) and the preosteoblast cell line MC3T3-E1 (preosteoblast) were treated with varying concentrations of zoledronate (ZOL). Viability was measured after 72 hours by MTT assay. Results are normalized as percentage of control. **b**, The preosteoblast cell line MC3T3-E1 were cultured in osteogenic supplement with indicated concentrations of ZOL. Alizarin red was used to identify mineralized area. Results are normalized to vehicle-treated controls. **c-d**, Plots of functional forms used to represent the osteoblast mineralization time (**c**) and the fold change to osteoclast lifespan (**d**) with indicated concentrations of ZOL. **e**, Interaction diagram of normal bone cells with ZOL.

1977   Red line denotes inhibition, black like indicates stimulation. **f-h**, Computational outputs of

1978   bone area to total area ratio (**f**), cumulative number of osteoclasts (**g**), and units of bone

1979   resorbed per osteoclast (**h**) following treatment of normal bone model with indicated

1980   concentrations of ZOL. Treatment begins on day 365 (black dotted line) and is

1981   applied continuously for 3 years, *** $p<0.001$, **** $p<0.0001$.

1982

Supplementary Fig. 5. Myeloma alters bone microarchitecture *in vivo*. a-d, Tumor burden in tibia and femur was assessed by GFP positivity by flow cytometry in U266-bearing mice. High resolution microCT was used to assess trabecular number (Tb.N; **a**), thickness (Tb.Th; **b**) and spacing (Tb.Sp; **c**) and degree of connectivity (Conn.D; **d**).

Supplementary Fig. 6. Multiple myeloma alters bone marrow microenvironment. a-b, Tumor naïve or U266GFP-bearing mice were sacrificed on indicated days to identify and localize αSMA+ mesenchymal stromal cells (gold; **a**), osterix+ preosteoblasts (pink; **b**) and GFP+ U266 cells (green; **a-b**) by immunofluorescence. Scale bars = 50µm **c**, Brightfield images of TRAcP+ multinucleated osteoclasts (red) and ALP+ cuboidal bone-lining osteoblasts (blue). Scale bars = 100µm. Images correspond with quantifications from Figure 6.

2000

2001 **Supplementary Fig. 7. PI-sensitive MM cells outgrow their PI-resistant counterparts**

2002 **under normal growth conditions**. **a-b**, PI-sensitive U266 and PI-resistant PSR MM cell

2003 lines were grown in standard culture conditions, the number of cell number was recorded

2004 using trypan blue staining over 120h (**a**) and used to calculate doubling times (**b**).

2005 Proteasome inhibitor sensitive GFP expressing U266 MM cells were incubated at

2006 indicated ratios with their proteasome inhibitor RFP expressing counterparts (PSR) . The

2007 percentage of each population under vehicle control conditions was monitored over time

2008 using real time imaging microscopy (Incucyte). In parallel the impact of BTZ (4nM) on the

2009 outgrowth of the populations was observed revealing the emergence of the resistant

2010 population over time.

2011

2012

2013 **Supplementary Fig. 8. EMDR increases rate of myeloma relapse and tumor**
2014 **heterogeneity under pulsed bortezomib treatment.** Pulsed BTZ treatment (2 weeks
2015 on therapy, 1 week off) was applied to HCA model when MM burden reached 10% of the
2016 marrow. **a-b**, Tumor growth (**a**) for individual simulations (n = 25 per condition) and
2017 Kaplan Meier plots of rate of relapse (**b**) for pulsed BTZ therapy were calculated when p_Ω
2018 = 10^{-4} (left column) and p_Ω = 10^{-3} (right column).

2019

2020

Supplementary Fig. 9. EMDR increases tumor heterogeneity under continuous and pulsed bortezomib treatment. Continuous BTZ treatment (left column) or Pulsed BTZ treatment (2 weeks on therapy, 1 week off; middle and right column) were applied to HCA model when MM burden reached 10% of the marrow. **a-c**, The proportion of sensitive/resistant MM cells at end point (MM = 20% of the marrow; **a**) and tumor heterogeneity (**b-c**) were assessed with two resistance probabilities (left and middle columns, $p_\Omega = 10^{-4}$, right column $p_\Omega = 10^{-3}$) in the presence or absence of EMDR. **b**, Muller

2028   plots indicating resistant subclones arising in tumor, created using EvoFreq[62]. Each color

2029   represents a unique subclone. Red arrow indicates start of treatment. **c.** Mean number of

2030   resistant sub-clones arising in tumors that reached 20% and contained

2031   resistant subclones (MM/MA) following continuous or pulsed BTZ treatment at different

2032   locations within the BME with/without EMDR. 'Both' refers to resistant subclones that

2033   arise close to MSCs and BDFs. Overall, EMDR leads to significantly higher numbers of

2034   resistant subclones.

2035

Supplementary Fig. 10. The impact of select parameter values on key model outputs. Continuous BTZ treatment was applied to HCA model when MM burden reached 10% of the marrow. **a.** Proportion of tumors that survived (lighter shade) or relapsed (darker shade) was assessed as resistance probability increased. **b-e**. Select parameters were varied to assess how the relapse time (when MM burden reached 20% of the marrow) and proportion of sensitive cells at endpoint changed due to parameter

2043　values ($p_\Omega = 10^{-4}$). MM_EMDR_DEATH is the lifespan of sensitive cells (+ BTZ) protected

2044　by EMDR (**b**). MAX_RESISTANT_DIVISION_RATE is the maximum division time of

2045　resistant cells (+/- BTZ) (**c**). MM_DEATH_BDF is the lifespan of sensitive cells (-BTZ) or

2046　resistant cells (+/- BTZ) in the presence of BDF (**d**). MAX_MM_DIVISION_RATE is

2047　the maximum division time of sensitive cells (+/- BTZ) in the presence of

2048　MSC/preosteoblast (**e**). The star marker indicates the outputs corresponding to the

2049　baseline parameter value. The circular marker indicates the mean value of the outputs

2050　with error bars representing the standard deviation of the simulations (n = 25); the size of

2051　the circular marker increases as the proportion of simulations that reached the endpoint

2052　increased.

2053

2054

2055 **Supplementary Video 1. HCA model recapitulates normal bone remodeling.**

2056 HCA simulation of normal bone remodeling, showing agent grid (top) and PDE grids with
2057 scaled concentration of RANKL (bottom left) and bone derived factors (BDF, bottom right)
2058 over one year. Each bone remodeling event is initiated through a small microfracture,
2059 which creates a signal to osteoblast lineage cells to express
2060 RANKL. Preosteoclasts migrate to the bone remodeling site and undergo fusion in
2061 response to RANKL to become a fully formed osteoclast. As the osteoclast resorbs the
2062 bone, BDF is released from the bone matrix which promotes the proliferation
2063 of preosteoblasts. During the reversal period, BDF continues to be released at a lower
2064 level, causing the preosteoblasts to migrate and attach to the eroded surface. Low BDF
2065 promotes the differentiation of preosteoblasts into bone-forming osteoblasts,
2066 which continue to build bone until the amount of bone that was resorbed is replaced. The
2067 bone formation phase is then followed by a period of quiescence until bone remodeling
2068 is re-initiated at the given location.

2069 YouTube link: https://www.youtube.com/watch?v=UFpXzLNFMzo

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2072 **Supplementary Video 2. HCA model captures key steps of myeloma-bone vicious**
2073 **cycle.**

2074 HCA simulation of the myeloma-bone vicious cycle, showing agent grid (top) and PDE
2075 grids with scaled concentration of RANKL (bottom left) and bone derived factors (BDF,
2076 bottom right) over one year. Each simulation is initialized with a single MM cell after the
2077 formation of the first osteoclast. MM increases the number of osteoclasts which drives
2078 bone resorption and the release of BDFs. BDFs and MSCs that are recruited in response
2079 to MM contribute to the growth and survival of MM cells (light green cells), causing MM
2080 cells to further expand in the bone marrow. At the same time, MM cells inhibit the
2081 differentiation of MSCs and preosteoblasts, preventing the formation of bone and further
2082 driving osteolytic bone disease.

2083 YouTube link: https://www.youtube.com/watch?v=NFdpWp2l1wg

2084

2085

2086 **Supplementary Video 3. EMDR increases minimal residual disease.**

2087 HCA simulation of continuous treatment with bortezomib (BTZ), showing agent grid (top)

2088 and PDE grids with scaled concentration of RANKL (bottom left) and bone derived factors

2089 (BDF, bottom right). Treatment begins when multiple myeloma (MM) cells have reached

2090 10% of the bone marrow (the starting point of the supplemental video) and continues until

2091 the MM burden doubles. After treatment begins, MM cells have a probability of resistance

2092 (p_Ω) during cell division that causes resistance to BTZ. When $p_\Omega = 10^{-4}$, EMDR (middle)

2093 protected a portion of sensitive cells, enabling them to acquire resistance and drive tumor

2094 relapse. When EMDR is absent (right), the tumor went extinct.

2095

2096 YouTube link: https://www.youtube.com/watch?v=fnBuxXvWWXw

2097

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Supplementary Video 4. Higher resistance probability increases tumor relapse

rates in absence of EMDR.

HCA simulation of continuous treatment with bortezomib (BTZ), showing agent grid (top)

and PDE grids with scaled concentration of RANKL (bottom left) and bone derived factors

(BDF, bottom right). Treatment begins when multiple myeloma (MM) cells have reached

10% of the bone marrow (the starting point of the supplemental video) and continues until

the MM burden doubles. After treatment begins, MM cells have a probability of resistance

(p_Ω) during cell division that causes resistance to BTZ. When $p_\Omega = 10^{-3}$, EMDR (middle)

protected a portion of sensitive cells, enabling them to acquire resistance and drive tumor

relapse. When EMDR is absent (right), the high resistance probability prevents tumors

from going extinct before the acquisition of intrinsic resistance and also drives tumor

relapse.

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2112 YouTube link: https://www.youtube.com/watch?v=EJUOy0yepWw

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