Identifying content-invariant neural signatures of perceptual vividness

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1 Abstract

Some conscious experiences are more vivid than others. Although perceptual vividness is a key

component of human consciousness, how variation in this magnitude property is registered by the human

brain is unknown. A striking feature of magnitudes in other psychological domains, such as number or

reward, is the existence of neural magnitude codes that are independent from sensory contents. To test

whether perceptual vividness similarly covaries with neural codes that are invariant to sensory content,

we reanalysed existing MEG and fMRI data from two distinct studies, quantifying perceptual vividness

via subjective ratings of awareness and visibility. Using representational similarity and decoding analyses,

we find evidence for the existence of content-invariant neural codes for perceptual vividness distributed

across visual, parietal, and frontal cortices. Our findings are consistent with a hypothesis that the

subjective vividness of conscious experience is supported by neural signatures similar to magnitude codes

in other cognitive domains.

Significance Statement

The vividness of conscious experience varies across different stimuli and contexts. Despite being a fundamental feature of conscious awareness, exactly how perceptual vividness is encoded in the human brain remains unclear. Neural codes underpinning magnitude in reward and numerosity domains have been shown to be unchanging as stimulus identity varies. Here, we test whether components of neural activity covarying with the magnitude of perceptual vividness are similarly independent of perceptual content in analyses of MEG and fMRI data. We find dynamic, content-invariant neural signatures of vividness in visual, parietal, and frontal cortices. Our findings introduce the surprising notion that neural signatures of conscious experience might follow similar coding principles to those found for magnitude properties of entirely different cognitive domains.

Introduction

Humans are aware of their environment: we experience the sights and sounds of the world around us. Some experiences, however, are more vivid than others. For example, seeing a bird on a clear day will be more vivid than seeing one on a foggy evening. Similarly, a car alarm outside your office can be very vivid until your attention is consumed by a work task. The neural correlates of experience therefore naturally involve some representation of the magnitude of perceptual vividness. While the neural basis of perceptual vividness is yet to be systematically characterised, neural codes for magnitude quantities in other cognitive domains, such as reward and numerosity, are better understood. Many neural magnitude codes contain a content-invariant component, where the magnitude property is represented independently of its sensory features (Chib et al., 2009; McNamee et al., 2013; Piazza et al., 2007). For instance, the number "9" is represented as larger than the number "5", regardless of whether we are comparing 9 vs. 5 apples, oranges, or saxophones. Here, we ask whether similar magnitude properties of perceptual vividness are also invariant to stimulus content: i.e. is the difference in vividness between seeing a bird on a clear day versus on a foggy evening represented in a similar way as the difference in vividness between hearing a car alarm with or without attending to it? We investigate this question by testing the extent to which neural signatures associated with reports of perceptual vividness are independent of perceptual content.

Content-invariance is a well-established feature of several neural magnitude codes. In the orbitofrontal cortex, for example, common representations of reward magnitude are shared across vastly different reward identities (Chib et al., 2009; Howard et al., 2015; Klein-Flügge et al., 2013; McNamee et al., 2013; Padoa-Schioppa & Assad, 2006). Furthermore, presentation of the same numerosity elicits suppression effects across symbolic (Arabic numerals) and non-symbolic (dots) stimuli in the intraparietal lobe (Piazza et al., 2007), and multivariate cross-classification has revealed common representations of numerosity across

symbolic and non-symbolic formats too (Teichmann et al., 2018). Finally, in strong support for the content-

invariance of magnitude codes, there is also evidence that numerical and reward magnitudes (amongst

others) are encoded in a domain-general manner where, for example, higher numbers are represented

similarly to highly rewarding stimuli and lower numbers are represented similarly to stimuli with low

reward values, indicating a shared neural system underpinning representations of magnitude in both

domains (Luyckx et al., 2019; Summerfield et al., 2020; Walsh, 2003).

Given the evidence for the existence of content-invariant neural magnitude codes in other domains, it is

intriguing to ask whether invariance to perceptual content is also a feature of the neural activity covarying

with the magnitude of perceptual vividness. If perceptual vividness is only encoded in a content-specific

manner, our experience of a stimulus such as a red circle may become vivid through the increased firing of

neural populations representing this feature (Itti & Baldi, 2009) (Figure 1, left). However, if neural activity

covarying with perceptual vividness also contains a content-invariant component, we should be able to find

neural signatures of vividness that are independent of those covarying with sensory features. The drivers of

such content-invariant signals may include changes in attention, emotion, and other cognitive factors that

surpass stimulus-specific salience, but nevertheless contribute to the vividness of experience (Morales,

2018, 2021) – an idea consistent with philosophical positions that distinguish percepts from their 'force'

and 'vivacity' (Hume, 2000; Teng, 2022). As such, rather than being bound to content-specific

representations, perceptual vividness might also covary with neural activity in a domain-general fashion,

independently of stimulus content (Figure 1, right) (Levinson et al., 2021; Podvalny et al., 2019; Samaha

et al., 2017; Sanchez et al., 2020).

Figure 1. Hypothesised neural signatures of perceptual vividness. *Left: Content-specific neural signatures associated with perceptual vividness.* The subjective vividness of a red circle is associated with the strength of red circle-representing neurons while the vividness of a blue square is associated with the strength of blue square-representing neurons. The neural signatures underpinning the vividness of these two experiences are therefore different. *Right: Content-invariant neural signatures associated with perceptual vividness.* The subjective vividness of both red circles and blue squares is associated with the same neural signature, which supersedes the stimulus-specific neural activity. Attention, emotion, and other cognitive factors may drive this content-invariant neural signal of vividness. We note that the represented coding schemes are not mutually exclusive, and it is likely that both play a role in determining the vividness of perceptual experience.

To test whether the neural code for perceptual vividness contains a content-invariant component, we reanalysed both magnetoencephalography (MEG; Andersen et al., 2016) and functional magnetic resonance imaging (fMRI; Dijkstra et al., 2021) data to investigate how perceptual vividness is represented in the human brain. The difficulty in isolating pure correlates of vividness and awareness from co-varying neural

signals (e.g. those related to arousal or performance) is well-known, and we did not attempt to tackle these

issues here (Aru et al., 2012; Lau, 2022). Instead, we sought to determine the representational structure of

awareness and visibility reports about different stimulus contents, to ask whether neural signatures

covarying with vividness did so in a content-specific or content-invariant manner. To anticipate our results,

we found evidence that neural representations of perceptual vividness generalize over stimulus content,

exhibit a graded structure, and can be identified across visual, parietal, and frontal brain regions, consistent

with signatures of magnitude codes in other cognitive domains.

Materials and Methods

MEG experiment

To explore the structure and dynamics of abstract representations of awareness ratings, we re-analysed an MEG dataset previously acquired at Aarhus University (Andersen et al. 2016). The data were recorded in a magnetically shielded room using an Elekta Neuromag Triux system with 102 magnetometers and 204 orthogonal planar gradiometers. Data were recorded at a frequency of 1000 Hz.

Participants

Nineteen participants took part in the experiment (Mean age = 26.6 years; SD = 4.4 years). Two participants were excluded from our analyses: one for failing to complete the experiment and the other for not using the 'almost clear experience' rating at all (see procedure details below).

Experimental Design and Statistical Analyses

In order to obtain a range of awareness ratings from each subject, a visual masking paradigm was used (Figure 2A). First, a fixation cross was presented for either 500, 1000, or 1500 ms, followed by a target stimulus for 33.3 ms. The target stimulus was either a square or a diamond presented in white/grey on a black (RGB value 0, 0, 0) background (Figure 2B). A static random noise mask followed the target and was presented for 2000 ms. Participants were required to identify the target during these 2000 ms, before rating their awareness of the stimulus on the perceptual awareness scale (PAS). PAS consists of four possible responses: no experience (NE), weak glimpse (WG), almost clear experience (ACE), and clear experience (CE). Following identification of the target, participants reported their awareness of the stimulus. The response boxes used for target identification and awareness report were swapped between hands every 36 trials to minimise lateralised motor responses contributing to MEG activity patterns. More details regarding the instructions given to participants about each PAS response can be found in Andersen et al. (2016).

The experiment consisted of one practice block and 11 experimental blocks, each with 72 trials. A contrast

staircase was used for the target stimuli in order to obtain a sufficient number of responses for each PAS

rating. The staircase procedure had 26 contrast levels ranging from a contrast of 2% to 77%, with a step

size of 3 percentage points. In the practice block and first experimental block, the staircase increased by 1

level if a participant made an incorrect judgement on the identification task, and decreased by 2 levels if a

participant made 2 successive correct identification judgements. For the remainder of the blocks, the

staircase was adjusted based on which PAS rating the participant had used least throughout the experiment

so far. Specifically, if NE had been used the least number of times throughout a block, 3 levels were

subtracted after 2 consecutive correct answers, and 1 added for a wrong answer. If WG was the least used

response, 2 levels were subtracted and 1 added. For ACE, 1 level was subtracted and 2 added. For CE, 1

level was subtracted and 3 added. This staircase procedure ensured a sufficient number of responses for

each rating.

Figure 2. Experimental paradigms. A: Experimental paradigm for the MEG data collected by Andersen et al. (2016). First, a fixation cross was presented for 500, 1000 or 1500 ms. Then, either a square or a diamond was shown for 33.3 ms, followed by a static noise mask for 2000 ms. While the mask was shown, participants reported the identity of the target. Finally, they reported their awareness of the stimulus using the PAS scale. **B:** Stimuli used in Andersen et al. (2016). **C:** Experimental paradigm for the fMRI data collected by Dijkstra et al. (2021). A stimulus was presented for 17 ms, followed by a 66 ms ISI and a 400 ms mask. Participants then indicated whether the stimulus was animate or inanimate, and finally rated the visibility of the stimulus on a four-point scale. **D:** Stimuli used in Dijkstra et al. (2021).

Pre-processing

MEG data were analysed using MATLAB 2019a and FieldTrip (Oostenveld et al., 2011). The data were

pre-processed with a low pass filter at 100 Hz, as well as a Discrete Fourier Transform (DFT) and bandstop

filters at 50 Hz and its harmonics. The data were split into epochs of -200 to 2000 ms around stimulus onset

and down-sampled to 250 Hz. For baseline correction, for each trial, activity 200 ms prior to stimulus

presentation was averaged per channel and subtracted from the entire epoch. During artefact rejection, trials

with high variance were visually inspected and removed if they were judged to contain excessive artefacts.

This procedure was performed blind to the experimental condition to avoid experimenter bias and was

completed separately for the magnetometers and gradiometers in the Elekta Neuromag Triux system.

Following artefact rejection the mean number of trials per PAS rating were as follows (numbers in brackets

refer to standard deviations): No Experience: 180.35 (59.64); Weak Glimpse: 168.10 (74.75); Almost Clear

Experience: 186.35 (82.74); Clear Experience: 115.24 (77.13). To further remove eye-movement artefacts,

an independent components analysis was carried out on the MEG data, and the components with the highest

correlation with each of the electro-oculographic (EOG) signals were discarded after visual inspection.

Components showing topographic and temporal signatures typically associated with heart rate artefacts

were also removed by eye.

Since we re-analysed previously collected data, we were unable to fully control for neural signals that

typically covary with awareness level. As such, to better characterise the contribution of these signals to

ratings of awareness we created two additional analysis pipelines. First, to ensure our results were not

entirely driven by the contrast level of the stimuli, we regressed stimulus contrast level on each trial out of

the pre-processed MEG data. Second, to investigate whether differences in pre-stimulus activity contributed

to differences in perceptual visibility (Benwell et al., 2017; Podvalny et al., 2019; Samaha et al., 2017) we

ran our data through the same pre-processing pipeline as above except for two adjustments: removing the

baseline correction stage and lengthening the epochs to -450 ms to 2000 ms around stimulus presentation.

The omission of baseline correction allows the analysis to be sensitive to differences in the pre-stimulus

activity (in the offset or mean amplitude, for example) of trials associated with different awareness ratings

which would otherwise be removed by baseline correction (the baseline correction procedure results in each

trial's pre-stimulus window having a mean activity of zero across all time points for each channel, such that

our RSA and decoding analyses would be unable to detect and characterise any pre-stimulus contribution

to visibility codes).

Representational similarity analysis

Representational similarity analysis (RSA) allows us to directly compare bespoke hypotheses about the

structure of neural data (Kriegeskorte & Kievit, 2013). In RSA, hypotheses are expressed as model

representational dissimilarity matrices (RDMs), which define the predicted similarity of neural patterns

between different conditions according to each hypothesis. In our case, we defined 4 model RDMs that

make different predictions about whether or not awareness ratings generalise over perceptual content, and

whether or not each rating leads to a graded activation pattern partially shared by neighbouring ratings

(Figure 3A).

In our Abstract-Graded RDM, we model awareness ratings as being independent of perceptual content

(such that ratings of a clear experience of a square have an identical neural profile to those of a clear

experience of a diamond), as well as being graded in nature (exhibiting a distance effect such that ratings

of "no experience" are more similar to those of "weak glimpse", than of "almost clear experience"). In the

Specific-Graded RDM, awareness ratings are modelled as being graded in the same way, but they are now

represented differently depending on which specific stimulus they are related to. Conversely, the Abstract-

Discrete RDM represents PAS ratings as independent of perceptual content but with no graded

structure/distance effects (such that the neural code underpinning a report of "no experience" is equally

(dis)similar to the neural code reflecting either a "weak glimpse" or a "clear experience"). Finally, the

Specific-Discrete RDM reflects our null model, whereby there is no observable representational similarity

structure among conditions, such that neural patterns reflecting one specific awareness rating are equally

dissimilar to all other awareness ratings.

RSA involves the comparison of the model RDMs with empirical RDMs constructed from neural data. To

do this, we first ran a linear regression on the MEG data with dummy coded predictors for each of our eight

conditions (Square trials: NE, WG, ACE, CE; Diamond trials: NE, WG, ACE, CE; trial condition coded

with a 1, alternative classes coded with a 0). This resulted in coefficient weights for each condition at each

time point and sensor, with the weights representing the neural response per condition, averaged over trials.

We then computed the Pearson distance between each pair of condition weights over sensors, resulting in

an 8 x 8 neural RDM reflecting the similarity of neural patterns across different awareness ratings and

stimulus types (Luyckx et al., 2019). Neural RDMs were subsequently smoothed over time via convolution

with a 60 ms uniform kernel.

We then compared this neural RDM with our model RDMs. To compare model RDMs with the neural

RDM, we correlated the lower triangle of the model and neural RDMs using Kendall's Tau rank correlation

(Nili et al., 2014). We performed this procedure at every time point, resulting in a correlation value at each

time point for each model. Importantly, we only correlated the lower triangle of the RDMs, excluding the

diagonal to avoid spurious correlations driven by the increased similarity of on-diagonal values compared

to off-diagonal values (Ritchie et al., 2017). This precluded us from directly testing our Specific-Discrete

model, since it is represented by a uniform RDM, and as such would give identical rank correlation values

regardless of the neural RDM it was compared to. However, since this RDM reflects our null model (i.e.

that there is no observable representational structure amongst awareness ratings), this model is implicitly

compared with the other model RDMs when we examine whether the correlation of these model RDMs

with the neural RDM is greater than 0.

One concern with this approach is that the graded hypotheses may win due to the neural data itself being

noisy. In other words, if a classifier is unable to cleanly separate distinct ratings, there will be greater overlap

between all ratings in the empirical RDM, including those of close neighbours. To ensure we did not obtain

spuriously high similarity with the Abstract-Graded model in virtue of this model's low-frequency content,

we performed a shuffling and blending procedure. This procedure involved shuffling the lower triangle of

the Abstract-Discrete RDM before apportioning neighbours of the four (shuffled) high correlation cells

with graded amounts of correlation. Correlation was blurred most to immediate neighbours, and less to

diagonal neighbours, matching the format of the graded RDMs (Figure 3C). We ran this procedure 1000

times per subject, resulting in 1000 Shuffled-Discrete and 1000 Shuffled-Graded RDMs. We compared all

shuffled-discrete and shuffled-graded RDMs with subjects' neural data at each time point. Finally, we took

the average correlation value for each time point across all permutations such that we had a Kendall's Tau

value for both the Shuffled-Discrete and Shuffled-Graded RDMs across time per subject. Through this

approach, we were able to compare neural data with RDMs that shared no representational similarity with

our Abstract-Graded RDM while controlling for differences in variance and frequency profile.

Within-subject multivariate decoding analysis

To support and extend conclusions drawn from our RSA analyses, we ran an exploratory analysis using

temporal generalisation methods (King & Dehaene, 2014) to identify content-invariant and graded

representations of awareness ratings while also investigating the stability of these representations over

time. In this procedure, a separate classifier is trained on each time point (from 200 ms pre-stimulus to

2000 ms post-stimulus) and tested on all other time points. This method results in a time-by-time

decoding accuracy matrix indicating the extent to which neural representations are stable over time.

Above chance decoding at a particular point in the decoding matrix indicates that neural representations

present at the training and testing time points are similar, whilst chance decoding indicates the

representations have changed.

We ran the above temporal generalisation analysis using both a within-condition and cross-condition

decoding procedure. Within-condition decoding involved training and testing the decoder to classify PAS

ratings on trials from one stimulus type (either squares or diamonds). In cross-condition decoding, we

trained on trials from one stimulus type and tested on trials from the other (e.g. trained on square trials

and tested on diamond trials, and vice-versa). In both cases, we used a 5-fold cross validation scheme,

with a balanced number of trials per class within each fold. Cross-condition decoding, where a classifier

trained to decode multivariate neural patterns in one class of stimuli is tested on an unseen class of

stimuli, offers an empirical test of whether the neural patterns associated with each class share a similar

neural code across conditions (Albers et al., 2013; Bernardi et al., 2020; Dijkstra et al., 2018). This

analysis therefore complements the RDM analysis in being able to test for content-invariant perceptual

visibility codes, while also providing information about their stability over time. We performed all

multiclass decoding analyses with a multiclass Linear Discriminant Analysis (LDA) decoder using the

MVPA-light toolbox (Treder, 2020) with FieldTrip. Each of the four PAS ratings served as classes for the

decoder to classify trials into. We used L1-regularisation of the covariance matrix, with the shrinkage

parameter calculated automatically using the Ledoit-Wolf formula within each training fold (Ledoit &

Wolf, 2004).

It is important to note that cross-validation is not technically necessary during cross-condition decoding

because the test data is never seen by the classifier during training, so there is no risk of overfitting.

However, we employed a cross-validation scheme for all our decoders so that differences in their

performance would not be due to differences in training procedures (e.g. number of trials in the training or

test set). Data was smoothed over 7 samples (28ms) and classification analysis was run on individual time

points throughout the whole trial to characterise the temporal dynamics of the representations (-200 to 2000

ms post-stimulus).

Stimulus decoding

One difficulty with interpreting a content-invariant representation of perceptual visibility is that it may

reflect a lack of power to detect content-specific differences between conditions (e.g. square vs. diamond).

To control for this possibility, we sought to ensure that the resolution of our data was sufficiently fine-

grained to pick up differences in the neural encoding of different stimuli. To do this, we applied a binary

decoding procedure using a binary LDA decoder with the same classification parameters as above. In this

analysis, the two stimulus types (squares and diamonds) were used as classes for the decoder to classify

trials into. For this analysis we grouped trials into low (NE and WG) and high visibility (ACE and CE)

trials to ensure sufficient power, performing the decoding analysis separately in each group. Once again,

data were smoothed over 7 samples (28ms) and analysed on individual time points throughout the whole

trial (-200 to 2000 ms post-stimulus).

Statistical Inference

To determine whether our RSA and decoding results were statistically significant, we used cluster-based

permutation testing (Maris & Oostenveld, 2007) with 1000 permutations. For RSA, within each

permutation we flipped the sign of each ranked correlation value at each time point for each participant and

performed a one-sample t-test against 0. Resulting t-values associated with a p-value smaller than 0.05 were

used to form clusters across the single time dimension. For each cluster, an associated cluster statistic was

computed, the largest of which was stored per permutation to build a group-level null distribution. The

cluster statistic computed from our observed data was then compared to this chance distribution to

determine statistical significance with an alpha level of 0.05. This procedure controls for the multiple

comparisons problem by only performing one comparison at the inference stage and specifically tests the

null hypothesis that the observed data are exchangeable with data from the permuted (null) distribution

(Maris & Oostenveld, 2007). We used the same cluster-based permutation procedure to compare how well

different model RDMs predicted the neural data. In this case, we performed paired-comparisons where

ranked correlation values per RDM were randomly swapped within subjects per permutation to build up a

group-level null distribution.

For decoding results, we used the same cluster-forming parameters, but this time randomly flipped the sign

of individual subjects' accuracy scores per permutation to build up a group-level null distribution.

Additionally, we formed clusters over both time dimensions of the temporal generalisation matrices. We

used the same cluster-based permutation procedure to compare performance between cross-condition and

within-condition decoders.

It is important to note that our cluster-based permutation testing procedure does not allow for inference as

to the exact time points at which neural representations come into existence. This is because the algorithm

does not consider individual time points at the statistical inference stage, since at this point it only relies on

cluster statistics, which encompass multiple time points (Sassenhagen & Draschkow, 2019). Still, as we are

not interested in the precise onset of content-invariant representations of awareness ratings but rather their

general temporal profile, this method is sufficient for our purposes.

fMRI experiment

To help localise representations of perceptual visibility in the brain, we re-analysed a previously collected

fMRI dataset (Dijkstra et al., 2021). It is worth noting that, while source-space decoding in MEG is certainly

possible (Andersen et al., 2016; Sandberg et al., 2013), fMRI is much better suited to answering this

question at a fine spatial scale, especially as we wish to compare the (potentially fine-grained) differences

and similarities in regional activity covarying with perceptual content and/or visibility.

Participants

Thirty-seven participants took part in the study. Eight participants were excluded from our analyses. One

was excluded because they quit the experiment early, and another because they failed to follow task

instructions. The final six subjects were excluded because they did not have at least 10 trials in each

visibility rating class after our grouping procedure (see *Within-subject multivariate searchlight decoding*

analysis below). Twenty-nine subjects were thus included in our final analyses (mean age = 25.35; SD =

6.31).

Stimuli

The stimuli used were taken from the POPORO stimulus data set (Kovalenko et al., 2012). The stimuli

selected were a rooster, a fish, a watering can, and a football (Figure 2D), and were selected based on

familiarity and visual difference to maximise classification performance as well as both accuracy and

visibility scores calculated in a pilot experiment run by Dijkstra et al. (2021). The mask was created by

randomly scrambling the pixel values of all stimuli combined (Figure 2C).

Experimental Design and Statistical Analyses

The experiment consisted of two tasks: a perception task and an imagery task. Each of these tasks were

executed in interleaved blocks and were counterbalanced across participants. Our re-analysis used data only

from the perception task and thus we omit details of the imagery component of the study. The perception

task ran as follows. A stimulus was presented for 17 ms, followed by a backward mask for 400 ms.

Participants then indicated whether the stimulus was animate or inanimate and rated the visibility of the

stimulus on a scale from 1 (not visible at all) to 4 (perfectly clear). Button response mappings were

counterbalanced across trials. The task was made up of visible and invisible trials. The difference between

these trials was the length of the interstimulus interval (ISI) between the stimulus and the mask. In the

visible trials the ISI was 66 ms, and in the invisible trials the ISI was 0 ms. In the present study, we only

analysed data from invisible trials (Figure 2C) because these were associated with the variation in the

visibility ratings that we are interested in. Choosing to focus on a single ISI also means that differences in

visibility ratings were not driven by differences in stimulus presentation characteristics. There were 184

trials in total, with 46 repetitions per stimulus divided over 4 blocks. More detailed information regarding

the study protocol can be found in (Dijkstra et al., 2021).

Acquisition

fMRI data were recorded on a Siemens 3T Skyra scanner with a Multiband 6 sequence (TR: 1 s; voxel size:

2 x 2 x 2 mm; TE: 34 ms) and a 32-channel head coil. The tilt of each participant's field of view was

controlled using Siemens AutoAlign Head software, such that each participant had the same tilt relative to

their head position. T1-weighted structural images (MPRAGE; voxel size: 1 x 1 x 1 mm; TR: 2.3 s) were

also acquired for each participant.

Preprocessing

Data were pre-processed using SPM12 (RRID: SCR_007037). Motion correction (realignment) was

performed on all functional imaging data before co-registration to the T1 structural scan. The scans were

then normalised to MNI space using DARTEL normalisation and smoothed with a 6 mm Gaussian kernel,

which has been shown to improve group-level decoding accuracy (Gardumi et al., 2016; Hendriks et al.,

2017; Misaki et al., 2013). Slow signal drift was removed using a high pass filter of 128s.

General Linear Model

Coefficient weights were estimated per trial with a general linear model that contained a separate regressor

for each trial at the onset of the stimulus convolved with the canonical HRF. Alongside nuisance regressors

(average WM and CFG signals and motion parameters), the screen onset and button press of both the

animacy and visibility responses were included as regressors, as well as a constant value per run to control

for changes in mean signal amplitude across runs.

Within-subject multivariate searchlight decoding analysis

For decoding our fMRI data, we binarized the visibility ratings into low and high visibility classes. This is

because in contrast to the MEG experiment, visibility was not staircased per-participant, leading to a large

number of participants failing to have enough trials at each of the four visibility ratings in both animate and

inanimate trials. Because training a decoder on such a small number of trials would yield unreliable and

noisy results, trials were therefore sorted into low visibility and high visibility classes on a subject-by-

subject basis prior to analysis. This was performed as follows. The median visibility rating (from 1 to 4)

was extracted from each subject and trials with a lower visibility rating than the median were classed as

low visibility trials, and those with visibility ratings equal to or greater than the median were classed as

high visibility trials. This procedure allowed us to control for the fact that different subjects had different

distributions of visibility ratings, such that the lower 1 and 2 ratings did not always correspond to low

visibility trials, and likewise the higher 3 and 4 ratings did not always correspond to high visibility trials.

For instance, one subject may have used visibility ratings 2 and 3 in around 50% of trials, rating 4 on the

other 50%, and not used rating 1 at all. In this case, we would label ratings 2 and 3 as low visibility, and

rating 4 as high visibility.

Trials were next grouped according to whether they contained an animate or inanimate stimulus. For each

participant, if there were less than 10 trials in either the low or high visibility class for either the animate or

inanimate trials, the participant was removed. This was the case for 6 participants. The mean number of

trials per condition following this procedure were as follows (numbers in brackets denote the standard

deviation): animate-high visibility: 63.48 (11.34); animate-low visibility: 25.31 (10.38); inanimate-high

visibility: 61.10 (12.24); inanimate-low visibility: 28.86 (11.48).

We used an LDA classifier on the beta estimates per trial to decode low and high visibility ratings within

and across animate/inanimate stimulus conditions. Cross-condition decoding was performed by training the

LDA classifier on low versus high visibility ratings in animate trials and then testing it on low versus high

visibility ratings in inanimate trials, and vice versa. Cross-condition decoding was performed with the same

logic as in our MEG analysis: if we train a classifier to decode visibility ratings in animate trials and use

this classifier to successfully decode visibility ratings in inanimate trials, we can conclude the

representations of visibility ratings are similar across different perceptual content. Once again, we also

performed within-condition decoding, where the classifier was trained on low versus high ratings in one

condition (e.g., animate trials), and tested on trials in the same condition allow a direct comparison of

within- and across-condition decoding performance. This comparison allowed us to determine where

content-specific representations of perceptual visibility may exist in the brain. Decoding was performed

with a 5-fold cross validation scheme using L1 regularisation with a shrinkage parameter of 0.2, and, similar

to the MEG analysis, cross-validation was used for both within-condition and cross-condition decoding.

Trials were down-sampled prior to decoding, such that there was an equal number of low and high visibility

trials in each fold. To ensure that our data were sensitive enough to show content-specific codes, we

additionally ran a similar analysis that sought to decode stimulus content (animate or inanimate) rather than

visibility. This analysis was similar in structure except the classifier was trained to decode animate vs.

inanimate trials rather than visibility level.

Decoding was performed using a searchlight method. Searchlights had a radius of 4 voxels (257 voxels per

searchlight). As such, at every searchlight the classifier was trained on 257 features (one beta estimate for

each voxel in the searchlight) for each trial in every fold. The searchlights moved through the brain

according to the centre voxel, meaning that each voxel was entered into multiple searchlights. After

decoding in each searchlight, the accuracy of the classifier was averaged across folds and this value was

stored at the centre of the searchlight to produce a brain map of decoding accuracy.

Stimulus decoding in fMRI Regions of Interest (ROI)

As in the MEG analysis, we again wished to establish that findings of content-invariant awareness

representations were not due to an inability to decode content itself. We tested our ability to decode

perceptual content within two ROIs with successful visibility decoding from our searchlight results. To do

this, we created two masks, one visual and one frontal, and then selected the 200 voxels within this mask

that had the highest mean visibility decoding accuracy averaged across all four decoding directions (within

animate; within inanimate; train animate-test inanimate; train inanimate-test animate). For the frontal mask

we used a connectivity-based parcellation of the orbitofrontal cingulate cortex that spanned frontal regions

with successful visibility decoding (8m and 32d; (Neubert et al., 2015), whereas our visual mask spanned

an area with successful visibility decoding in occipital regions (VO1, VO2, PHC1, and PHC2; (Wang et

al., 2015). Using the 200 ROI voxels as features, we decoded animate (rooster and fish) versus inanimate

(watering can and football) stimuli in low and high visibility trials separately using the same 5-fold cross

validation procedure and LDA parameters as above, down-sampling trials prior to decoding to ensure an

equal number of animate and inanimate trials in each fold.

Group-level statistical inference

Distributions of accuracy values from classification of fMRI data are often non-Gaussian and asymmetric

around chance level. This means that parametric statistical comparisons, such as t-tests against chance

decoding (50%), are unable to provide valid tests of whether group-level accuracy values are significant

(Stelzer et al., 2013). Therefore, to determine where classifiers had performed significantly above chance,

we compared mean performance across all participants with a null distribution created by first permuting

the class labels 25 times prior to decoding per participant and then using bootstrapping to form a group-

level null distribution of 10,000 bootstrapping samples (Stelzer et al., 2013). We did this separately for each

decoding direction (within: train and test on animate; train and test on inanimate; cross: train on animate,

test on inanimate; train on inanimate, test on animate). To perform statistical inference on an average cross-

decoding map created by averaging the two cross-condition decoding directions, this average map was

compared to a group-level null distribution formed by averaging the two null distributions created for the

two separate maps. To compare within-condition and cross-condition classification performance, a group-

level null distribution was formed by taking the difference between cross and within decoding scores

throughout the bootstrapping procedure. To control for multiple comparisons in the searchlight analysis,

resulting p values were subsequently corrected for multiple comparisons with a false discovery rate of 0.01.

Results

Representational structure of perceptual visibility in whole-brain MEG data

We used RSA to test whether perceptual visibility levels (PAS ratings) correlated with MEG activity

patterns independently of perceptual content (Abstract RDMs) or together with perceptual content (Specific

RDMs). We additionally tested whether neural activity patterns covaried with visibility levels in a graded

or discrete manner (Figure 3A). A model instantiating graded and abstract representations of awareness

ratings significantly predicted the neural data throughout most of the post-stimulus period (purple line;

Figure 3B). In contrast, a model with an abstract but discrete representational structure was able to predict

the neural data only in an early phase of the trial between approximately 100 to 500 milliseconds after

stimulus onset (green line). Paired comparisons between these two models showed that the Abstract-Graded

model was significantly better at predicting the neural data than the Abstract-Discrete model throughout

the majority of the trial (purple and green dots). The Specific-Graded model did not significantly predict

the neural data at any point during the trial (gold line), and likewise the Abstract-Graded model was found

to be significantly better at predicting the neural data than the Specific-Graded model in a direct comparison

(purple and yellow dots), indicating that an abstract model of awareness ratings better described their neural

representation. To assess the spatial distribution of Abstract-Graded signals across sensors, we repeated the

analysis for frontal and occipital sensors separately (following Hu et al., 2018), finding similar results in

each case (Figure 3S1). These results indicate that neural correlates of perceptual visibility generalise over

perceptual content and exhibit distance effects, indicative of neural populations tuned to specific degrees

of visibility with overlapping tuning curves.

To ensure that the neural data did not exhibit spuriously high similarity with the Abstract-Graded model in

virtue of its increased variance and reduced frequency when compared to the Abstract-Discrete and Specific

models, we performed a shuffling and blending control analysis (Figure 3C). This procedure revealed no

significant prediction of the neural data for either the shuffled-discrete or shuffled-graded RDMs (Figure

3D). As such, RDMs with frequency and variance profiles matching that of the Abstract-Graded RDM, but

without any relationship with awareness ratings, were not able to significantly predict neural data, in

contrast to the Abstract-Graded model that captures the graded and content-invariant structure of awareness

ratings. To additionally control for the possible influence of stimulus contrast on our RDM results, we

confirmed that similar results were obtained when regressing out the linear component of contrast (Figure

3S2). It is possible that nonlinear or multivariate effects of contrast may have still driven some of our

findings, but as the source of variation in visibility is less important for our main question about content-

invariance, we did not pursue this further.

Figure 3. Neural representations of perceptual visibility are abstract and graded. A: *From left to right:*

Abstract-Graded model where neural correlates of awareness ratings are independent of perceptual content

and follow a graded structure; Abstract-Independent model where awareness ratings are independent of

perceptual content but do not follow a graded structure; Specific-Graded model where awareness ratings

are specific to the perceptual content to which they relate and follow a graded structure; Specific-Discrete

(Null hypothesis) model where there is no observable representational structure amongst awareness ratings

(PAS ratings, NE: No Experience, WG: Weak Glimpse, ACE: Almost Clear Experience, CE: Clear

Experience). **B**: RSA reveals that the Abstract-Graded model was the best predictor of the representational

structure of neural patterns in whole-brain sensor-level MEG data. Solid horizontal lines represent time

points significantly different from 0 for a specific RDM at $p < .05$, corrected for multiple comparisons.

Horizontal dots denote statistically significant paired comparisons between the different models at $p < .05$,

corrected for multiple comparisons. We obtained similar findings across occipital (Figure 3S1A) and frontal

(Figure 3S1B) sensors separately, as well as in datasets with stimulus contrast level regressed out (Figure

3S2) and without baseline correction (Figure 3S4). We also examined the pattern of classifier mistakes

during cross-stimulus decoding, again revealing distance-like effects in perceptual visibility decoding

(Figure 3S3). **C:** Shuffling and blending procedure. This analysis was performed to control for naturally

occurring low-frequency content in neural data. **D:** Results from both shuffled models reflect the average

Kendall's Tau over 1000 shuffling permutations. Purple, red, and blue lines represent similarity of the

Abstract-Graded, shuffled-discrete, and shuffled-graded models respectively with neural data. The

shuffled-discrete line varies only slightly from 0 and is thus hard to see. The Abstract-Graded model is the

only model under consideration that significantly predicted the neural data.

To further characterize the graded representational structure of perceptual visibility, we computed

confusion matrices between each rating and its neighbours. By plotting the proportion of predictions for

each awareness rating made by the multiclass classifier separately for trials of each rating, we can visualise

when our decoder makes mistakes, and which PAS ratings it most often confuses (Figure 3S3). These

confusion plots confirm the distance effects identified with the RSA model comparison, in which

neighbouring PAS ratings are most often confused with each other by the classifier, and more distant ratings

less so, suggesting that visibility is represented in a graded, ordinal manner.

Finally, we asked whether our model RDMs could also predict pre-stimulus neural activity. If a graded,

abstract structure for perceptual visibility is already evident prior to stimulus presentation, this would be

indicative of trial-to-trial fluctuations in attention or arousal contributing to our ability to decode content-

invariant visibility signals. Interpreting (a lack of) pre-stimulus decoding from our previous RSA analyses

is confounded by the baseline correction procedure applied during pre-processing. To address this issue,

we re-ran our analysis on data that had not been baseline corrected. We found that pre-stimulus activity was

not captured by any of the candidate RDMs, and that stimulus-triggered responses continued to show the

same graded/abstract pattern of results as in our initial analysis (Figure 3S4). Together these results indicate

that pre-trial fluctuations in attention and/or arousal are unlikely to drive our results.

Temporal profile of perceptual visibility codes

Next, we performed a temporal generalisation analysis to further unpack the content-invariant nature of

neural signatures of perceptual visibility and to characterize how and whether their patterns change from

timepoint to timepoint. Off-diagonal panels in Figure 4 (top right and bottom left) depict temporal

generalisation matrices for both directions of cross-condition decoding (top-right: train on squares-test on

diamonds; bottom-left: train on diamonds-test on squares). Within these panels, above-chance decoding on

the major diagonal indicates that representations of visibility begin to show content-invariance from just

after stimulus onset up until the moment of report. Contrasting cross-condition decoding with within-

condition decoding resulted in no significant differences in decoding accuracy for either comparison (train

on squares, test on diamonds vs. within squares: all $p > 0.89$; train on diamonds, test on squares vs. within

diamonds: all $p > 0.4$). In other words, we did not find any evidence that there was content-specific visibility

information available over and above content-invariant information. Furthermore, the lack of off-diagonal

decoding in each temporal generalisation matrix indicates that the format of content-invariant neural

signatures of visibility change rapidly over time.

Figure 4. Abstract representations of perceptual visibility evolve rapidly over time. Main figure: Temporal generalisation results for the classification of PAS ratings from MEG data (4 PAS responses; chance = 0.25). For each row, statistical comparisons between the two columns showed no significant differences in decoding accuracy between within- and cross-condition decoding. Non-translucent regions within solid lines highlight above chance decoding, as revealed by cluster-based permutation tests. We replicated these findings in non-baseline-corrected data (Figure 4S1).

We again replicated this analysis in a dataset that had not undergone baseline correction to test whether activity contributing to participants' awareness ratings could be decoded prior to stimulus presentation. In

line with our RSA analysis on this dataset, we could not decode awareness ratings prior to stimulus

presentation when data had not been baseline-corrected (Figure 4S1).

Content-invariant representations of visibility are found across visual, parietal, and frontal cortex

To localise brain regions supporting content-invariant representations of perceptual visibility, we re-

analysed an existing fMRI dataset (Dijkstra et al., 2021). We used a searchlight approach to identify brain

regions that represent perceptual visibility in an abstract manner. Both cross-condition and within-condition

decoding resulted in above chance accuracy in a number of regions across the visual, parietal, and frontal

cortex (Figure 5). To assess whether representations of perceptual visibility were stimulus-dependent in

certain areas of the brain, we compared cross-condition decoding to within-condition decoding in both

animate and inanimate trials (training on animate trials vs. within animate trials; training on inanimate trials

vs. within inanimate trials), and found no significant differences. In other words, we found no evidence that

stimulus-specific visibility information was present over and above stimulus-invariant visibility

information. See Table S1 for details of the clusters of accuracy scores found to be significantly above

chance in both cross-condition and within-condition decoding analyses.

Figure 5. Abstract representations of perceptual visibility are found across visual, parietal, and

frontal cortex. Searchlight decoding in fMRI data revealed significantly above chance accuracy in both

cross and within-condition decoding of visibility ratings. Clusters of successful decoding were found across

large regions of the frontal, parietal, and visual cortex. Our statistical comparison of cross and within-

condition decoding accuracy revealed no significant differences anywhere in the brain. Significance was

assessed at p < .05, corrected for multiple comparisons with an FDR of 0.01. Clusters are reported in Table

S1.

Stimulus content can be decoded from both MEG and fMRI data

We next considered the possibility that a content-invariant neural signature of visibility may be obtained

because of insufficient sensitivity to perceptual content in our dataset. To address this, we sought to

decode stimulus identity, rather than visibility level. Stimulus decoding was above chance in both datasets

for high visibility trials. In the MEG data, we were able to decode stimulus identity (square vs. diamond)

in trials in which participants used the upper two PAS ratings (ACE/CE), but not when participants used

the lower two PAS ratings (NE/WG; Figure 6A). Similarly, in the fMRI data, the decoding of animate vs.

inanimate stimuli was significantly above chance in a visual cortical ROI during trials reported as high

visibility (mean accuracy = 0.52; p = 0.007) but not in trials reported as low visibility (mean accuracy =

0.496; p = 0.655; Figure 6B). It was not possible to decode stimulus content from a frontal cortical ROI in

either low (mean accuracy = 0.5; p = 0.406) or high visibility trials (mean accuracy = 0.507; p = 0.159).

Together, these analyses indicate that stimulus content could be reliably decoded in posterior visual

regions.

Stimulus Content and Visibility are Encoded in Dissociable Brain Regions

Although perceptual content could be decoded from high visibility trials (Figure 6A, 5B), it is still unclear

how these content representations relate to the abstract decoding of stimulus visibility (Figure 5). For

instance, it may be that abstract signals reflecting visibility, particularly in the visual cortex, arise from

distinct content-specific representations sharing features that covary with visibility.

To further probe the relationship between neural signatures of content and visibility, we ran a searchlight

decoding procedure to decode animate versus inanimate stimuli in our fMRI data. Since content could

only be decoded in high visibility trials in our ROI analysis (Figure 6B), we restricted the analysis to

these trials. We then compared the overlap between the content-decoding searchlight and the content-

invariant visibility searchlight maps. To do this we computed mean content cross-decoding accuracy

averaged over the two cross-decoding directions (train on animate, test on inanimate; train on inanimate,

test on animate) prior to group-level inference (see Methods).

Overall, there was minimal overlap between representations of content and visibility (Figure 6C). Despite

overlapping clusters being obtained in the superior and inferior lateral occipital cortex (see Table S2 for

full list of individual and overlapping clusters), clear anatomical distinctions in occipital regions can be

seen between representations of stimulus content and visibility, with the former being decoded from more

lateral regions of the occipital cortex, while the latter was decoded closer to the medial surface (Figure

6C, Table S2). As expected, fewer clusters of above-chance stimulus content decoding were found in

frontal regions, whereas content-invariant representations of visibility were more abundant in these areas

(Hatamimajoumerd et al., 2022). Distinct decoding patterns for content and visibility representations

further strengthens the notion that content-invariant representations of visibility exist partly independently

of perceptual content, even in regions typically associated with the encoding of stimulus content such as

the visual cortex (Kamitani & Tong, 2005; Kriegeskorte et al., 2008; Mazor et al., 2022).

Figure 6. Perceptual content can be decoded in high visibility trials and shows distinct

representations to visibility decoding. A: Decoding of perceptual content on each trial (squares or

diamonds) from participants' whole-brain sensor-level MEG data for low visibility (NE and WG) and

high visibility (ACE and CE) trials separately. Successful decoding was possible in high visibility trials

up to approximately 700ms post-stimulus onset. Lines are smoothed using a Gaussian-weighted moving

average with a window of 20 ms. Shaded area denotes 95% confidence intervals. The solid horizontal line

reflects above-chance decoding, as revealed by cluster-based permutation tests. **B**: Decoding of perceptual

content on each trial (animate or inanimate) from participants' fMRI data for low visibility and high

visibility trials separately. Decoding was successful in a visual ROI in high but not low visibility trials,

and unsuccessful in a frontal ROI. Asterisks denote significance at p < .01. Error bars illustrate 95%

confidence intervals. **C:** Searchlight decoding accuracy for content decoding in high visibility trials (blue)

and for content-invariant visibility decoding (red). Clusters illustrate areas where content or content-

invariant visibility could be decoded significantly above chance. Content-invariant representations of

visibility were more widespread than content representations and extended into the prefrontal cortex,

whereas both content and visibility could be decoded in distinct locations of the visual cortex.

Significance was assessed at $p < .05$, corrected for multiple comparisons with an FDR of 0.01. Clusters

are reported in Table S2.

Discussion

In this study we asked whether perceptual vividness covaries with neural activity patterns in a content-specific or content-invariant manner. By applying multivariate analyses to MEG and fMRI datasets in which participants rated their awareness of visual stimuli, we found that the vividness of experience is represented in a similar way across different stimulus contents and exhibits signatures of an ordered and graded magnitude code. Furthermore, neural representations of perceptual vividness change rapidly over time and are localized across visual, parietal, and frontal cortices.

The identification of content-invariant representations of perceptual vividness (Figure 3) is in line with recent work highlighting a dissociation between neural correlates of awareness and perceptual content. For example, Sanchez et al. (2020) found neural patterns that indicated whether an individual was aware of a stimulus or not, irrespective of which sensory modality it was presented in. Likewise, Mazor et al. (2022) reported that, while stimulus identity was best decoded from occipital regions, perceptual vividness could be effectively decoded from a wider range of areas including the parietal and frontal cortex. Notably, a recent study also found that graded changes in perceptual vividness could be reliably decoded from the prefrontal cortex, even in the absence of report, consistent with a contribution to the vividness of experience (Hatamimajoumerd et al., 2022). Here we build on these findings by showing that the structure of neural signals underlying graded awareness ratings – ranging from the absence of an experience of particular content, to a clear and vivid experience – are content-invariant.

Our finding that neural representations of awareness ratings display a distance effect (Figure 3; Figure 3S3) is suggestive of perceptual vividness relying on similar schemes to those encoding magnitude in other domains such as number. Specifically, our results are consistent with the possibility that distributed populations of neurons are tuned to specific phenomenal magnitudes, in the same way that specific

populations of neurons are sensitive to certain numerical magnitudes (Harvey et al., 2013; Kutter et al.,

2018; Piazza et al., 2004). Such a prediction could be tested through repetition suppression experiments

(Piazza et al., 2004), and/or by collecting single-unit recordings from human patients while they provide

subjective awareness ratings (Pereira et al., 2021). A variety of analogue magnitudes have been shown to

rely on common magnitude representations (Luyckx et al., 2019; Pinel et al., 2004; Yallak & Balcı, 2021),

prompting a hypothesis that domain-general representations are responsible for encoding low-dimensional

quantities in the brain (Summerfield et al., 2020; Walsh, 2003). Therefore, an intriguing possibility is that

perceptual vividness is supported by similar domain-general magnitude codes. Future work could explore

this hypothesis by assessing whether representations of vividness share neural resources with other

analogue magnitude codes such as those for reward or number (Luyckx et al., 2019).

The existence of stimulus-independent representations of perceptual vividness in visual cortical areas

(Figure 5) was unexpected, since these areas have been shown to distinguish stimulus features rather than

subjective vividness in previous studies (Kamitani & Tong, 2005; Kriegeskorte et al., 2008; Mazor et al.,

2022). One concern is that neural representations of vividness ratings as revealed by decoding analyses may

look similar across stimuli if content-specific information encoded in separate neural populations is treated

as belonging to the same population (i.e. within the same voxel). Successful cross-stimulus decoding of

vividness ratings could then occur by way of decoding the amplitude of (content-specific) neural responses

in these voxels (Fisch et al., 2009; Moutoussis & Zeki, 2002). As a step towards addressing this concern,

we show that stimulus-specific decoding remains possible specifically in visual areas on high- (but not low)

visibility trials (Figure 5A; Figure 5B), suggesting that the abstract nature of perceptual vividness

representations in this region is not due to a lack of power to detect stimulus-specific effects. Moreover, we

show anatomical distinctions between content and visibility encoding (Figure 6C), again indicating that the

unexpected above-chance decoding of visibility in the visual cortex is unlikely to be an artefact of a failure

to detect content-specific representations.

Another possibility is that content-invariant signals of perceptual vividness in visual cortex reflect pre-

stimulus activations that have been shown to contribute to participants' awareness level in previous studies

(Podvalny et al., 2019). Here we could not identify pre-stimulus contributions to visibility codes in our

MEG data (Figure 4S2), supporting a hypothesis that the content-invariant and graded representations we

report here are largely stimulus-triggered. As such our results suggest that the content-invariant signals

related to awareness level in the current data are partly distinct to those reported by Podvalny *et al*. in

temporal profile. In any case, it is worth noting that fluctuations in (pre-stimulus) attention and arousal

affecting the intensity of experience (as well as other psychological factors like emotional state or

motivation) should not necessarily be seen as orthogonal to perceptual vividness signals. Indeed, in certain

accounts of consciousness, there is a close relationship between attention-like processes (e.g. the monitoring

of the precision or reliability of first-order perceptual content (Feldman & Friston, 2010)), and the

phenomenal magnitude attached to that content (Lau, 2019; Fleming, 2020; Graziano, 2013).

By applying temporal generalisation analysis to our MEG data, we were able to reveal the dynamics of

vividness representations over time. This analysis indicated that neural patterns covarying with perceptual

vividness are unstable, changing during the course of a trial (Figure 4), consistent with a sequence of

different neural populations correlating with awareness level over time (King & Dehaene, 2014). Given

that we find that vividness is tracked across a variety of cortical regions, such a rapidly changing temporal

profile may reflect dynamic message passing between distinct neural populations, consistent with the

reverberation of predictions and prediction errors in hierarchical generative models. Future work to directly

test this hypothesis could leverage informational connectivity analyses (e.g. Seeliger et al., 2021) to

determine the direction of information flow across interacting brain regions, or use RSA to combine M/EEG

and fMRI data collected using the same task and stimuli (Cichy et al., 2014).

In summary, we show that perceptual vividness covaries with content-invariant neural representations that

exhibit graded distance effects similar to those observed for analogue magnitude codes in other cognitive

domains. These representations are spatially distributed and rapidly evolve over time, consistent with the

flow of awareness-related information across the visual, parietal, and frontal cortices. This pattern of

results adds to growing evidence for a content-invariant neural component contributing to the strength of

conscious experience.

Data Availability Statement

All code is available at the following GitHub Repository: https://github.com/benjybarnett/abstract-

awareness. fMRI data is accessible at https://doi.org/10.34973/j9yn-q419 and MEG data will be made

available upon acceptance.

References

Albers, A. M., Kok, P., Toni, I., Dijkerman, H. C., & de Lange, F. P. (2013). Shared Representations

for Working Memory and Mental Imagery in Early Visual Cortex. *Current Biology*, *23*(15),

1427–1431. https://doi.org/10.1016/J.CUB.2013.05.065

Andersen, L. M., Pedersen, M. N., Sandberg, K., & Overgaard, M. (2016). Occipital MEG Activity

in the Early Time Range (<300ms) Predicts Graded Changes in Perceptual Consciousness.

Cerebral Cortex, *26*(6), 2677–2688. https://doi.org/10.1093/cercor/bhv108

Aru, J., Bachmann, T., Singer, W., & Melloni, L. (2012). Distilling the neural correlates of

consciousness. *Neuroscience and Biobehavioral Reviews*, *36*(2), 737–746.

https://doi.org/10.1016/j.neubiorev.2011.12.003

Benwell, C. S. Y., Tagliabue, C. F., Veniero, D., Cecere, R., Savazzi, S., & Thut, G. (2017).

Prestimulus EEG Power Predicts Conscious Awareness But Not Objective Visual

Performance. *ENeuro*, *4*(6). https://doi.org/10.1523/ENEURO.0182-17.2017

Bernardi, S., Benna, M. K., Rigotti, M., Munuera, J., Fusi, S., & Salzman, C. D. (2020). The

Geometry of Abstraction in the Hippocampus and Prefrontal Cortex. *Cell*.

https://doi.org/10.1016/j.cell.2020.09.031

Chib, V. S., Rangel, A., Shimojo, S., & O'Doherty, J. P. (2009). Evidence for a Common

Representation of Decision Values for Dissimilar Goods in Human Ventromedial

Prefrontal Cortex. *Journal of Neuroscience*, *29*(39), 12315–12320.

https://doi.org/10.1523/JNEUROSCI.2575-09.2009

Cichy, R. M., Pantazis, D., & Oliva, A. (2014). Resolving human object recognition in space and

time. *Nature Neuroscience*, *17*(3), 455–462. https://doi.org/10.1038/nn.3635

Dijkstra, N., Gaal, S. van, Geerligs, L., Bosch, S. E., & Gerven, M. A. J. van. (2021). No Evidence

for Neural Overlap between Unconsciously Processed and Imagined Stimuli. *ENeuro*,

8(5), ENEURO.0228-21.2021. https://doi.org/10.1523/ENEURO.0228-21.2021

Dijkstra, N., Mostert, P., de Lange, F. P., Bosch, S., & van Gerven, M. A. J. (2018). Differential

temporal dynamics during visual imagery and perception. *ELife*, *7*, 1–16.

https://doi.org/10.7554/eLife.33904

Fisch, L., Privman, E., Ramot, M., Harel, M., Nir, Y., Kipervasser, S., Andelman, F., Neufeld, M. Y.,

Kramer, U., Fried, I., & Malach, R. (2009). Neural 'Ignition': Enhanced Activation Linked

to Perceptual Awareness in Human Ventral Stream Visual Cortex. *Neuron*, *64*(4), 562–

574. https://doi.org/10.1016/j.neuron.2009.11.001

Gardumi, A., Ivanov, D., Hausfeld, L., Valente, G., Formisano, E., & Uludağ, K. (2016). The effect

of spatial resolution on decoding accuracy in fMRI multivariate pattern analysis.

NeuroImage, *132*, 32–42. https://doi.org/10.1016/J.NEUROIMAGE.2016.02.033

Harvey, B. M., Klein, B. P., Petridou, N., & Dumoulin, S. O. (2013). Topographic Representation

of Numerosity in the Human Parietal Cortex. *Science*, *341*(6150), 1123–1126.

https://doi.org/10.1126/science.1240405

Hatamimajoumerd, E., Ratan Murty, N. A., Pitts, M., & Cohen, M. A. (2022). Decoding

perceptual awareness across the brain with a no-report fMRI masking paradigm. *Current*

Biology. https://doi.org/10.1016/j.cub.2022.07.068

Hendriks, M. H. A., Daniels, N., Pegado, F., & Op de Beeck, H. P. (2017). The Effect of Spatial

Smoothing on Representational Similarity in a Simple Motor Paradigm. *Frontiers in*

Neurology, *0*(MAY), 222. https://doi.org/10.3389/FNEUR.2017.00222

Howard, J. D., Gottfried, J. A., Tobler, P. N., & Kahnt, T. (2015). Identity-specific coding of future

rewards in the human orbitofrontal cortex. *Proceedings of the National Academy of*

Sciences, *112*(16), 5195–5200. https://doi.org/10.1073/pnas.1503550112

Hu, Y., Yin, C., Zhang, J., & Wang, Y. (2018). Partial least square aided beamforming algorithm in

magnetoencephalography source imaging. *Frontiers in Neuroscience*, 616.

Hume, D. (2000). *1739. A treatise of human nature, ed. DF Norton and MJ Norton*. Oxford:

Oxford University Press.

Itti, L., & Baldi, P. (2009). Bayesian surprise attracts human attention. *Vision Research*, *49*(10),

1295–1306. https://doi.org/10.1016/j.visres.2008.09.007

Kamitani, Y., & Tong, F. (2005). Decoding the visual and subjective contents of the human brain.

Nature Neuroscience, *8*(5), 679–685. https://doi.org/10.1038/nn1444

King, J.-R., & Dehaene, S. (2014). Characterizing the dynamics of mental representations: The

temporal generalization method. *Trends in Cognitive Sciences*, *18*(4), 203–210.

https://doi.org/10.1016/J.TICS.2014.01.002

Klein-Flügge, M. C., Barron, H. C., Brodersen, K. H., Dolan, R. J., & Behrens, T. E. J. (2013).

Segregated Encoding of Reward–Identity and Stimulus–Reward Associations in Human

Orbitofrontal Cortex. *Journal of Neuroscience*, *33*(7), 3202–3211.

https://doi.org/10.1523/JNEUROSCI.2532-12.2013

Kovalenko, L. Y., Chaumon, M., & Busch, N. A. (2012). A pool of pairs of related objects

(POPORO) for investigating visual semantic integration: Behavioral and

electrophysiological validation. *Brain Topography*, *25*(3), 272–284.

https://doi.org/10.1007/S10548-011-0216-8

Kriegeskorte, N., & Kievit, R. A. (2013). Representational geometry: Integrating cognition,

computation, and the brain. *Trends in Cognitive Sciences*, *17*(8), 401–412.

https://doi.org/10.1016/J.TICS.2013.06.007

Kriegeskorte, N., Mur, M., Ruff, D. A., Kiani, R., Bodurka, J., Esteky, H., Tanaka, K., & Bandettini,

P. A. (2008). Matching Categorical Object Representations in Inferior Temporal Cortex of

Man and Monkey. *Neuron*, *60*(6), 1126–1141.

https://doi.org/10.1016/j.neuron.2008.10.043

Kutter, E. F., Bostroem, J., Elger, C. E., Mormann, F., & Nieder, A. (2018). Single Neurons in the

Human Brain Encode Numbers. *Neuron*, *100*(3), 753-761.e4.

https://doi.org/10.1016/j.neuron.2018.08.036

Lau, H. (2022). *In consciousness we trust: The cognitive neuroscience of subjective experience*.

Oxford University Press.

Lau, H., Michel, M., LeDoux, J. E., & Fleming, S. M. (2022). The mnemonic basis of subjective

experience. *Nature Reviews Psychology*. https://doi.org/10.1038/s44159-022-00068-6

Ledoit, O., & Wolf, M. (2004). A well-conditioned estimator for large-dimensional covariance

matrices. *Journal of Multivariate Analysis*, *88*(2), 365–411.

https://doi.org/10.1016/S0047-259X(03)00096-4

Levinson, M., Podvalny, E., Baete, S. H., & He, B. J. (2021). Cortical and subcortical signatures of

conscious object recognition. *Nature Communications*, *12*(1).

https://doi.org/10.1038/s41467-021-23266-x

Luyckx, F., Nili, H., Spitzer, B., & Summerfield, C. (2019). Neural structure mapping in human

probabilistic reward learning. *ELife*, *8*. https://doi.org/10.7554/eLife.42816

Maris, E., & Oostenveld, R. (2007). Nonparametric statistical testing of EEG- and MEG-data.

Journal of Neuroscience Methods, *164*(1), 177–190.

https://doi.org/10.1016/j.jneumeth.2007.03.024

McNamee, D., Rangel, A., & O'Doherty, J. P. (2013). Category-dependent and category-

independent goal-value codes in human ventromedial prefrontal cortex. *Nature*

Neuroscience, *16*(4), 479–485. https://doi.org/10.1038/nn.3337

Misaki, M., Luh, W. M., & Bandettini, P. A. (2013). The effect of spatial smoothing on fMRI

decoding of columnar-level organization with linear support vector machine. *Journal of*

Neuroscience Methods, *212*(2), 355–361.

https://doi.org/10.1016/J.JNEUMETH.2012.11.004

Morales, J. (2018). *The strength of the mind: Essays on consciousness and introspection*.

Columbia University.

Morales, J. (2021). Introspection Is Signal Detection. *The British Journal for the Philosophy of*

Science. https://doi.org/10.1086/715184

Moutoussis, K., & Zeki, S. (2002). The relationship between cortical activation and perception

investigated with invisible stimuli. *Proceedings of the National Academy of Sciences of*

the United States of America, *99*(14), 9527–9532.

https://doi.org/10.1073/pnas.142305699

Neubert, F. X., Mars, R. B., Sallet, J., & Rushworth, M. F. S. (2015). Connectivity reveals

relationship of brain areas for reward-guided learning and decision making in human

and monkey frontal cortex. *Proceedings of the National Academy of Sciences of the*

United States of America, *112*(20), E2695–E2704.

https://doi.org/10.1073/pnas.1410767112

Nili, H., Wingfield, C., Walther, A., Su, L., Marslen-Wilson, W., & Kriegeskorte, N. (2014). A

Toolbox for Representational Similarity Analysis. *PLoS Computational Biology*, *10*(4).

https://doi.org/10.1371/journal.pcbi.1003553

Padoa-Schioppa, C., & Assad, J. A. (2006). Neurons in the orbitofrontal cortex encode economic

value. *Nature*, *441*(7090), 223–226. https://doi.org/10.1038/nature04676

Pereira, M., Megevand, P., Tan, M. X., Chang, W., Wang, S., Rezai, A., Seeck, M., Corniola, M.,

Momjian, S., Bernasconi, F., Blanke, O., & Faivre, N. (2021). Evidence accumulation

relates to perceptual consciousness and monitoring. *Nature Communications*, *12*(1),

Article 1. https://doi.org/10.1038/s41467-021-23540-y

Piazza, M., Izard, V., Pinel, P., Le Bihan, D., & Dehaene, S. (2004). Tuning curves for approximate

numerosity in the human intraparietal sulcus. *Neuron*, *44*(3), 547–555.

https://doi.org/10.1016/j.neuron.2004.10.014

Piazza, M., Pinel, P., Le Bihan, D., & Dehaene, S. (2007). A Magnitude Code Common to

Numerosities and Number Symbols in Human Intraparietal Cortex. *Neuron*, *53*(2), 293–

305. https://doi.org/10.1016/j.neuron.2006.11.022

Pinel, P., Piazza, M., Le Bihan, D., & Dehaene, S. (2004). Distributed and overlapping cerebral

representations of number, size, and luminance during comparative judgments. *Neuron*,

41(6), 983–993. https://doi.org/10.1016/S0896-6273(04)00107-2

Pinheiro-Chagas, P., Piazza, M., & Dehaene, S. (2019). Decoding the processing stages of mental

arithmetic with magnetoencephalography. *Cortex*, *114*, 124–139.

https://doi.org/10.1016/j.cortex.2018.07.018

Podvalny, E., Flounders, M. W., King, L. E., Holroyd, T., & He, B. J. (2019). A dual role of

prestimulus spontaneous neural activity in visual object recognition. *Nature*

Communications, *10*(1), 1–13. https://doi.org/10.1038/s41467-019-11877-4

Ritchie, J. B., Bracci, S., & Op de Beeck, H. (2017). Avoiding illusory effects in representational

similarity analysis: What (not) to do with the diagonal. *NeuroImage*, *148*(January), 197–

200. https://doi.org/10.1016/j.neuroimage.2016.12.079

Samaha, J., Iemi, L., & Postle, B. R. (2017). Prestimulus alpha-band power biases visual

discrimination confidence, but not accuracy. *Consciousness and Cognition*, *54*, 47–55.

https://doi.org/10.1016/j.concog.2017.02.005

Sanchez, G., Hartmann, T., Fuscà, M., Demarchi, G., & Weisz, N. (2020). Decoding across

sensory modalities reveals common supramodal signatures of conscious perception.

Proceedings of the National Academy of Sciences, *117*(13), 7437–7446.

https://doi.org/10.1073/pnas.1912584117

Sandberg, K., Bahrami, B., Kanai, R., Barnes, G. R., Overgaard, M., & Rees, G. (2013). Early Visual

Responses Predict Conscious Face Perception within and between Subjects during

Binocular Rivalry. *Journal of Cognitive Neuroscience*, *25*(6), 969–985.

https://doi.org/10.1162/jocn_a_00353

Sassenhagen, J., & Draschkow, D. (2019). Cluster-based permutation tests of MEG/EEG data do

not establish significance of effect latency or location. *Psychophysiology*, *56*(6), 1–8.

https://doi.org/10.1111/psyp.13335

Seeliger, K., Ambrogioni, L., Gucluturk, Y., Van Den Bulk, L. M., Guclu, U., & Van Gerven, M. A. J.

(2021). End-to-end neural system identification with neural information flow. *PLoS*

Computational Biology, *17*(2), 1–22. https://doi.org/10.1371/JOURNAL.PCBI.1008558

Stelzer, J., Chen, Y., & Turner, R. (2013). Statistical inference and multiple testing correction in

classification-based multi-voxel pattern analysis (MVPA): Random permutations and

cluster size control. *NeuroImage*, *65*, 69–82.

https://doi.org/10.1016/j.neuroimage.2012.09.063

Summerfield, C., Luyckx, F., & Sheahan, H. (2020). Structure learning and the posterior parietal

cortex. *Progress in Neurobiology*, *184*, 101717.

https://doi.org/10.1016/j.pneurobio.2019.101717

Teichmann, L., Grootswagers, T., Carlson, T., & Rich, A. N. (2018). Decoding Digits and Dice with

Magnetoencephalography: Evidence for a Shared Representation of Magnitude. *Journal*

of Cognitive Neuroscience, *30*(7), 999–1010. https://doi.org/10.1162/jocn_a_01257

Teng, L. (2022). A metacognitive account of phenomenal force. *Mind & Language*, 1–21.

https://doi.org/10.1111/mila.12442

Treder, M. S. (2020). MVPA-Light: A Classification and Regression Toolbox for Multi-

Dimensional Data. *Frontiers in Neuroscience*, *0*, 289.

https://doi.org/10.3389/FNINS.2020.00289

Tsouli, A., Harvey, B. M., Hofstetter, S., Cai, Y., van der Smagt, M. J., te Pas, S. F., & Dumoulin, S.

O. (2021). The Role of Neural Tuning in Quantity Perception. *Trends in Cognitive*

Sciences, *xx*(xx), 1–14. https://doi.org/10.1016/j.tics.2021.10.004

Van Vugt, B., Dagnino, B., Vartak, D., Safaai, H., Panzeri, S., Dehaene, S., & Roelfsema, P. R.

(2018). The threshold for conscious report: Signal loss and response bias in visual and

frontal cortex. *Science*, *360*(6388), 537–542. https://doi.org/10.1126/science.aar7186

Vishne, G., Gerber, E. M., Knight, R. T., & Deouell, L. Y. (2022). *Representation of sustained*

visual experience by time-invariant distributed neural patterns (p. 2022.08.02.502469).

bioRxiv. https://doi.org/10.1101/2022.08.02.502469

Walsh, V. (2003). A theory of magnitude: Common cortical metrics of time, space and quantity.

Trends in Cognitive Sciences, *7*(11), 483–488. https://doi.org/10.1016/j.tics.2003.09.002

Wang, L., Mruczek, R. E. B., Arcaro, M. J., & Kastner, S. (2015). Probabilistic maps of visual

topography in human cortex. *Cerebral Cortex*, *25*(10), 3911–3931.

https://doi.org/10.1093/cercor/bhu277

Yallak, E., & Balcı, F. (2021). Metric error monitoring: Another generalized mechanism for

magnitude representations? *Cognition*, *210*.

https://doi.org/10.1016/j.cognition.2020.104532

 Supplemental Figures

Figure 2-figure supplement 1. Awareness Ratings Show Similar Representational Structure Across

Occipital and Frontal Sensors. RSA analysis performed over occipital sensors (top) and frontal sensors

(bottom) only. Purple, green, and gold lines represent similarity of the Abstract-Graded, Abstract-Discrete,

and Specific-Graded models respectively with neural data. Solid horizontal lines represent time points

significantly different from 0 for a specific RDM at $p < .05$, corrected for multiple comparisons. The

Abstract-Graded model significantly predicted the neural data throughout the majority of the trial (purple

line) across frontal sensors, and for a shorter duration when analysis was restricted occipital sensors only.

The Abstract-Discrete model was only successful at predicting the neural data across two clusters of time-

points post-stimulus when using occipital sensors, but was a significant predictor of neural data for larger

portions of the epoch when using frontal sensors. The Specific-Graded model did not significantly predict

the neural data at any time point in frontal or occipital sensors. Horizontal dots denote statistically

significant paired comparisons between the different models at $p < .05$, corrected for multiple comparisons.

Across frontal sensors, the Abstract-Graded model was a significantly better predictor of the neural data

than the Specific-Graded model, and likewise across the occipital sensors, both abstract models

significantly outperformed the Specific-Graded model. In this split-sensor analysis, the Abstract-Graded

model did not significantly outperform the Abstract-Specific model, however there was a noticeable trend

in the same direction as in the RSA performed across all sensors, where the difference in performance was

significant (Figure 2B).

 Figure 2 – figure supplement 2. RSA on MEG data with stimulus contrast level regressed out. When

983   stimulus contrast level was regressed out of the MEG data, an RSA still produced comparable results to

984   the original analysis. The Abstract-Graded model still predicted the neural data better than either

985   alternative model. Solid horizontal lines represent time points significantly different from 0 for a specific

986   RDM at p <.05, corrected for multiple comparisons. Horizontal dots denote statistically significant paired

987   comparisons between the different models at p <.05, corrected for multiple comparisons.

Figure 2 – figure supplement 3. Cross-decoding shows the graded nature of the PAS scale. For each

cross-condition decoder (A: Train on Squares; B: Train on Diamonds), the four sub-plots illustrate the

proportion of PAS ratings the classifiers decoded trials as. The subplots correspond to trials where the

true PAS rating reported by subjects were (from left to right) 'No Experience', 'Weak Glimpse', 'Almost

Clear Experience', and 'Clear Experience'. Each coloured line represents the proportion of trials

classified as each PAS rating across time. For example, in trials where participants reported No

Experience, the majority of trials were classified correctly (blue line), with the classifier most often

misclassifying these 'No Experience' trials as 'Weak Glimpse' ratings (orange line), and rarely

 misclassifying them as 'Almost Clear Experience' or 'Clear Experience' trials (gold and purple lines,

 respectively). Shaded areas represent 95% confidence intervals.

1000 **Figure 2 – figure supplement 4. RSA analysis for MEG data without baseline correction.** None of

1001 our model RDMs significantly predicted pre-stimulus activity in non-baseline-corrected data. Instead, the

1002 predominant neural signature was stimulus triggered, as in the main analysis (Figure 2B), with the

1003 Abstract-Graded model being the best predictor of neural representations of phenomenal magnitude.

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1009 **Figure 3 – figure supplement 2. Temporal Generalisation matrices for MEG decoding analyses on**

1010 **data without baseline-correction.** For each row, statistical comparisons between the two columns

1011 showed no significant differences in decoding accuracy between within and cross-condition decoding.

1012 Pre-stimulus decoding of awareness ratings was not possible, even when data had not been baseline-

1013 corrected.

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Decoding Type	Atlas Label	Cluster Size (voxels)	MNI Coordinates of maximum accuracy	Maximum accuracy
Cross (train animate)	Postcentral Gyrus	23,838	-46, -36, 54	0.593
Cross (train animate)	Temporal Fusiform Cortex	474	-31.5, -36.1, -25.8	0.567
Cross (train animate)	Paracingulate Gyrus	192	-8, 44, -6	0.563
Cross (train animate)	Frontal Orbital Cortex	168	-30, 34, -10	0.570
Cross (train animate)	Cingulate Gyrus, posterior division	109	4, -44, 10	0.563
Cross (train animate)	Occipital Pole	89	-22, -96, 2	0.562
Cross (train animate)	Frontal Pole	75	32, 36, -10	0.561
Cross (train animate)	Temporal Occipital Fusiform Cortex	59	20, -52, -18	0.566
Cross (train animate)	Lingual Gyrus	56	10, -38, -6	0.555
Cross (train animate)	Left Cerebral White Matter	56	-22, -38, 8	0.566
Cross (train inanimate)	Supramarginal Gyrus, anterior division	23,564	-54, -36, 30	0.593
Cross (train inanimate)	Subcallosal Cortex	512	5.85, 10.6, -6.63	0.575
Cross (train inanimate)	Left Caudate	176	-10, 2, 16	0.575

Cross (train inanimate)	Middle Temporal Gyrus, posterior division	166	-52, -42, -2	0.585
Cross (train inanimate)	Frontal Orbital Cortex	152	-32, 36, -12	0.570
Cross (train inanimate)	Left Hippocampus	106	-20, -16, -14	0.567
Cross (train inanimate)	Central Opercular Cortex	100	38, 0, 18	0.571
Cross (train inanimate)	Frontal Pole	78	22, 42, -12	0.565
Cross (train inanimate)	Insular Cortex	71	-38, -20, -4	0.564
Cross (train inanimate)	Lateral Occipital Cortex, superior division	62	32, -88, 14	0.555
Within (animate)	Cingulate Gyrus, anterior division	49,130	-2, 36, 20	0.616
Within (inanimate)	Postcentral Gyrus	32,710	62, -8, 18	0.601
Within (inanimate)	Right Caudate	79	18, 10, 16	0.565

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1020 **Table S1. fMRI Searchlight Decoding Results.** Clusters with above chance decoding of perceptual

1021 visibility for both cross-condition and within-condition decoding. Clusters are significant at p < .05,

1022 corrected for multiple comparisons with an FDR of 0.01. Region names are found for the peak co-ordinate

1023 using the Harvard-Oxford Cortical and Subcortical Structural Atlas.

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Decoding Type	Atlas Label	Cluster Size (voxels)	MNI Coordinates of maximum accuracy	Maximum accuracy
Content	Inferior Lateral Occipital Cortex	2768	-48, -70, -8	0.572
Content	Cerebellum	2150	0, -48, -10	0.558
Content	Inferior Frontal Gyrus	1837	-52, 32, 6	0.556
Content	Superior Lateral Occipital Cortex	919	-40, - 58, 54	0.557
Content	Superior Lateral Occipital Cortex	907	-8, -64, 60	0.554
Content	Angular Gyrus	735	44, -52, 20	0.557
Content	Superior Parietal Lobule	626	20, -44, 62	0.548
Content	Frontal Orbital Cortex	375	38, 24, -2	0.557
Content	Paracingulate Cyrus	371	-6, 26, 34	0.547
Content	Inferior Frontal Gyrus	356	46, 20, 20	0.563
Content	Superior Frontal Gyrus	209	16, 24, 58	0.546
Content	Frontal Pole	201	-24, 42, 44	0.546

Content	Superior Temporal Gyrus	192	-54, -2, -10	0.549
Content	Postcentral Gyrus	189	-62, -22, 38	0.547
Content	Posterior Cingulate Gyrus	178	-8, -26, 44	0.547
Content	Left Cerebral White Matter	133	6, -24, 16	0.544
Content	Cerebellum	98	34, -64, -40	0.547
Content	Superior Lateral Occipital Cortex	76	20, -66, 46	0.553
Content	Anterior Cingulate Gyrus	74	6, -4, 40	0.551
Content	Parietal Operculum Cortex	56	44, -32, 20	0.546
Content	Precentral Gyrus	52	44, -16, 58	0.542
Mean Cross-Condition Visibility	Precentral Gyrus	16,638	-50, 8 32	0.584
Mean Cross-Condition Visibility	Postcentral Gyrus	2863	-50, -30, 48	0.58
Mean Cross-Condition Visibility	Right Accumbens	278	10, 14, -6	0.561

Mean Cross-Condition Visibility	Left Cerebral White Matter	167	-16, 0, 16	0.568
Mean Cross-Condition Visibility	Frontal Medial Cortex	166	-4, 48, -10	0.555
Mean Cross-Condition Visibility	Middle Temporal Gyrus	150	-52, -42, -2	0.556
Mean Cross-Condition Visibility	Central Opercular Cortex	138	-36, -10, 18	0.563
Mean Cross-Condition Visibility	Frontal Orbital Cortex	133	32, 28, 2	0.556
Mean Cross-Condition Visibility	Occipital Fusiform Gyrus	116	14, -84, -22	0.557
Mean Cross-Condition Visibility	Cerebellum	103	-28, -42, -34	0.559
Mean Cross-Condition Visibility	Frontal Orbital Cortex	95	-36, 36, -10	0.563

Mean Cross-Condition Visibility	Temporal Occipital Fusiform Cortex	91	-40, -62, -24	0.554
Mean Cross-Condition Visibility	Inferior Lateral Occipital Cortex	58	42, -80, 4	0.553
Mean Cross-Condition Visibility	Frontal Pole	58	22, 38, -12	0.557
Mean Cross-Condition Visibility	Occipital Pole	56	12, -90, -2	0.557
Mean Cross-Condition Visibility	Superior Precentral Gyrus	53	26, -12, 52	0.552
Visibility and Content Overlap	Cerebellum	1587	-6, -82, -32	N/A
Visibility and Content Overlap	Frontal Orbital Cortex	1521	-28, 16, -24	N/A
Visibility and Content Overlap	Superior Lateral Occipital Cortex	782	-32, -74, 20	N/A
Visibility and Content Overlap	Precuneous Cortex	474	-14, -58, 18	N/A
Visibility and Content Overlap	Inferior Lateral Occipital Cortex	412	46, -68, -10	N/A

Visibility and Content Overlap	Supramarginal Gyrus	383	64, -28, 34	N/A
Visibility and Content Overlap	Frontal Pole	339	40, 36, 12	N/A
Visibility and Content Overlap	Cingulate Gyrus	315	0, 36, 16	N/A
Visibility and Content Overlap	Frontal Orbital Cortex	213	36, 22, -14	N/A
Visibility and Content Overlap	Middle Frontal Gyrus	181	-24, 36, 32	N/A
Visibility and Content Overlap	Posterior Cingulate Gyrus	156	-4, -30, 36	N/A
Visibility and Content Overlap	Middle Frontal Gyrus	147	24, 28, 34	N/A
Visibility and Content Overlap	Right Cerebral Cortex	145	20, 2, -14	N/A
Visibility and Content Overlap	Cerebellum	115	26, -58, -26	N/A
Visibility and Content Overlap	Cerebellum	111	-24, -36, -38	N/A
Visibility and Content Overlap	Superior Parietal Lobule	107	34, -50, 36	N/A
Visibility and Content Overlap	Postcentral Gyrus	101	-60, -20, 24	N/A

Visibility and Content Overlap	Postcentral Gyrus	74	-36, -22, 44	N/A
Visibility and Content Overlap	Lingual Gyrus	74	-14, -56, -2	N/A
Visibility and Content Overlap	Cerebellum	63	20, -72, -32	N/A
Visibility and Content Overlap	Cerebellum	52	34, -56, -48	N/A

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Table S2. fMRI Searchlight Content Decoding in High Visibility Trials, Average Cross-Condition

Visibility Decoding, and Overlapping Cluster Information. *Decoding type = Content*: Clusters with

above chance decoding of perceptual content (animate vs. inanimate) in high visibility trials. *Decoding*

type = Mean Cross-Condition Visibility: Clusters with above chance decoding of perceptual visibility for

cross-condition decoding when accuracy from both decoding directions (training on animate and training

on inanimate) was averaged together. To aid the identification of individual clusters in this map,

clustering was performed at an increased accuracy threshold of 0.54. *Decoding Type = Awareness and*

Content Overlap: Clusters where decoding of content and cross-decoding of visibility were both

successful (i.e. the intersection of the Content and Mean Cross-Condition Visibility clusters). Clusters are

significant at $p < .05$, corrected for multiple comparisons with an FDR of 0.01. Region names are found

for the peak co-ordinate using the Harvard-Oxford Cortical and Subcortical Structural Atlas and the MNI

Structural Atlas.