Cerebral oxygenation and cardiac output responses during short repeated sprints exercise

and modulatory effect of glucose ingestion

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New findings

1. How does cerebral oxy-, deoxy-, and total haemoglobin change during repeated

short cycling sprints.

2. Each repeated short sprints produce a transient increase in O_2Hb, HHb, and tHb,

which is positively correlated with cardiac output.

3. After each sprint, O_2Hb, HHb and tHb rapidly return to baseline, despite a still

elevated cardiac output.

4. Repeated sprints performance is accompanied with significant decrease in cerebral

haemoglobin saturation.

5. Glucose ingestion, although improving performance, does not affect O_2Hb, HHb, and

tHb responses to the repeated sprint exercise, but seems to enhance recovery of

cerebral tissue oxygenation after repeated sprint exercise.

Abstract

We studied the time profile of changes (Δ) in cerebral oxyhaemoglobin (O_2Hb),

deoxyhaemoglobin (HHb) and total haemoglobin (tHb) concentrations during the

performance of repeated sprints and its relationship with cardiac output. The modulatory

effect of glucose ingestion and acute hyperglycaemia on cerebral haemoglobin responses

was also investigated. Ten young male participants performed a set of 10 repeated 6-s

sprints on a cycle ergometer after ingesting 70 g of glucose (GLU) or a placebo drink (PLA).

Heart rate, stroke volume and cardiac output (impedance cardiography) and ΔO_2Hb, ΔHHb

and ΔtHb in the frontal region of the cerebral cortex using near-infrared spectroscopy (NIRS)

were continuously measured. Each sprint elicited a significant positive ΔO_2Hb and ΔHHb

response that was similar in the two trials. The magnitude of cerebral haemoglobin changes

increased with the number of sprint repetitions and was positively correlated with the

increase in cardiac output. After each sprint, O_2Hb and HHb rapidly returned to baseline,

while cardiac output remained elevated. At the end of the repeated sprints, O_2Hb decreased

to below pre-exercise values, whereas HHb and tHb were elevated. After 10-15 min

recovery, O_2Hb but not HHb or tHb, returned to pre-exercise values in the PLA, while in the

GLU trial O_2Hb increased above pre-exercise values (reactive hyperaemia). We conclude

that short sprint exercise induces elevation of O_2Hb, HHb and tHb during the sprint exertion

in parallel with the increase in cardiac output. However, together with the transient

increase in cerebral haemoglobin, a progressive decline in cerebral oxygen saturation

develops during the course of the repeated sprints. Glucose ingestion does not alter

cerebral haemoglobin responses to the sprint exercise but seems to be associated with a

faster recovery of O_2Hb.

Introduction

Studies measuring cerebral blood flow and blood flow velocity in the internal carotid or

middle cerebral artery reveal increased regional and global cerebral blood flow (CBF) during

dynamic exercise at moderate-to-severe exercise intensities [i.e., ~ 70% maximal oxygen

uptake ($\dot{V}O_{2max}$)] and a return of CBF toward baseline when work rate increases to maximal

exhaustive levels (Fisher et al., 2013; Hellstrom et al., 1996; Ide, Boushel, et al., 2000;

Jorgensen et al., 1992; Subudhi et al., 2008). Cerebral blood flow at rest and during exercise

is tightly regulated in response to changes in arterial blood gases (particularly carbon

dioxide), neural activity, blood pressure, and cardiac output (Ainslie et al., 2007; Hoiland et

al., 2016; Marsden et al., 2012; Ogawa et al., 2007; Ogoh, Brothers, et al., 2005). In parallel

with augmented CBF, cerebral metabolism also rises during dynamic exercise, as shown by

the observed decrease in cerebral metabolic ratio, or oxygen-to-carbohydrate index, due to

raised cerebral non-oxidative carbohydrate metabolism (Dalsgaard, 2006; Dalsgaard et al.,

2004; Ide et al., 1999). Such disparate increase in brain glucose and lactate uptake relative

to that of oxygen signals enhanced neural activity (Chuquet et al., 2010; Dienel, 2017; Dienel

& Cruz, 2016), and is typically observed during exhaustive exercise (Ide, Schmalbruch, et al.,

2000; Rasmussen et al., 2010), when exercise is performed in hyperthermic and hypoxic

conditions or when it is performed under increased mental effort (Dalsgaard et al., 2002).

Together with changes in CBF, dynamic exercise also affects cerebral tissue oxygenation

(Brassard et al., 2010; González-Alonso et al., 2004). The tissue concentration of

oxyhaemoglobin (O_2Hb) and deoxyhaemoglobin (HHb) can be determined non-invasively

and with a reasonable spatial resolution (~1-2 cm) using near-infrared spectroscopy (NIRS).

According to a meta-analysis of NIRS studies, during submaximal exercise, there is an

increase in blood volume and oxygen concentration in the frontal region of the cerebral

cortex, which is followed by a decline in cerebral oxygenation when exercise intensity

approaches maximal levels, suggestive of inadequate oxygen delivery relative to demand at

the end stages of incremental maximal exercise (Rooks et al., 2010). A recent systematic

review also reports that prefrontal cortex oxygenation rises with moderate-to-severe

intensity dynamic exercise due to increased O_2Hb and unchanged HHb, and declines when

exercise intensity increases to near-maximum or maximum intensity (De Wachter et al.,

2021). During graded exercise, the breakpoint leading to lowered cerebral oxygenation has

been shown to follow the respiratory compensation threshold with a short time lag, as a

consequence of cerebral vasoconstriction linked to compensatory hyperventilation-induced

hypocapnia (Bhambhani et al., 2007; Globus et al., 1983; Ogoh & Ainslie, 2009; Racinais et

al., 2014; Subudhi et al., 2008). The lowered cerebral oxygenation at near-maximal exercise,

combined with muscle deoxygenation, may impair muscle recruitment (Racinais et al., 2014)

and trigger fatigue, particularly when the exercise is undertaken under hypoxic conditions

(Subudhi et al., 2008).

Extreme short (<10 s) bouts of all-out sprint interval exercise is an attractive option for

achieving cardiorespiratory fitness (Shi et al., 2018), but compared to incremental maximal

exercise, the cerebrovascular response during this type of exercise is less documented. A

single study investigating cerebral oxygenation, arterial pressure, and cardiac output during

30-s all-out cycling exercise performed at normal ambient oxygen levels and in hypoxia

showed a linear decrease in middle cerebral artery blood flow velocity (MCAv) and a drop in

cerebral oxygenation level during the sprint that could only partially be explained by

changes in end-tidal carbon dioxide partial pressure ($P_{ET}CO_2$), suggesting that factors other

than hypocapnia regulate CBF during high-intensity exercise (Curtelin et al., 2018). Also, the

decrease in MCAv during the 30-s sprint occurred despite the substantial rise in cardiac

output and mean blood pressure (Curtelin et al., 2018). In another study, in which

participants performed seven 30-s exercise bouts on a cycle ergometer at a work rate of

150% maximal oxygen uptake, the brain's O_2Hb and total haemoglobin concentration (tHb)

increased during the first sprint, but with O_2Hb decreasing and HHb increasing from resting

levels in the last three sprint bouts, once again without a clear correlation between

cerebrovascular response and $P_{ET}CO_2$ (Shibuya et al., 2004). These two studies suggest that

contrary to submaximal and maximal exercise during supramaximal exercise CBF and

cerebral oxygenation are not strictly dependent on arterial CO_2 levels, blood pressure, and

cardiac output. However, 30-s sprints are very exhaustive, with high levels of fatigue and

severe drop in power output occurring during a single repetition of this exercise, which

could affect cerebrovascular responses. Therefore, the question remains of how cerebral

blood volume and oxygenation would change during shorter and repeated sprint efforts and

how such changes are related to cardiovascular responses and power output. Repeated

sprint-running elicits a high percentage of maximal oxygen uptake, high blood lactate levels,

and a cyclic pattern of changes in the difference between O_2Hb and HHb in the contracting

muscle whose dynamics follow the sprint/recovery time course (Buchheit et al., 2010), but

whether a similar pattern occurs in the brain has not been determined. Also, dynamic

cerebral autoregulation responds with a time delay similar to the duration of short sprint

bouts (~6 s) (Fantini et al., 2016), which may govern cerebral blood flow response during the

performance of a series of short sprints.

Blood glucose levels also determine cerebral metabolism and CBF (Xu et al., 2015). Although

glucose is the primary energy substrate utilized by the brain, acute hyperglycaemia has been

shown to decrease CBF and the cerebral metabolic rate of both oxygen and glucose

(Ishibashi et al., 2016; Xu et al., 2015), although opposite findings were reported (Tsuchida

et al., 2002). Hence, we also tested the effect of acute glucose intake and subsequent rise in

glycaemia in cerebral haemoglobin concentration changes during repeated sprints.

Therefore, this study aimed to investigate changes in cerebral O_2Hb, HHb, and tHb during

the performance of repeated cycling sprints and their relationship with both cardiac output

and power output. The effect of acute hyperglycaemia on cerebral (prefrontal) oxygenation

during the repeated sprint was also investigated. A NIRS probe scanning the entire

prefrontal cortex was used to assess brain oximetry, which allows compensating for

interindividual cerebral circulatory regional differences and to investigate differences in

cerebrovascular responses to short intermittent cycling sprints across the frontal region of

the cerebral cortex.

Methods

Participants and experimental design

Eleven healthy male adults volunteered (Table 1) to participate in this study after providing

written informed consent. Participants were free of any metabolic, cardiovascular, or

neurological disease and did not regularly participate in exercise training. The study protocol

was reviewed and approved by the ethics review board of the University of Macao (Special

Administrative Region of Macao, China) and conformed to the ethical principles for research

involving human participants (approved number: BSERE22-APP011-FED).

Each participant visited the laboratory on three separate occasions at least one week apart.

In the first visit, each participant performed a maximal incremental cycling exercise to

determine the individual $\dot{V}O_{2max}$. In the following visits, each participant performed a

repeated sprints exercise test on a cycle ergometer after ingesting 70 g of glucose (GLU) or a

taste-matched non-caloric placebo (PLA), in a randomised counterbalanced and single blind

design.

Instrumentation and measures

Maximal incremental test

The maximal incremental test was carried out on a cycle ergometer (Monark 839E, Varberg,

Sweden) to evaluate the individual $\dot{V}O_{2max.}$ After a warm-up at a workload of 25 W for 3 min,

participants started cycling at 50 W at a cadence of 60 ± 5 revolutions per minute (rpm),

with the workload increasing by 25 W every 3 min. The test was completed when the

participant reached volitional exhaustion, with a respiratory exchange ratio (RER) $\geq$ 1.15,

ratings of perceived exertion (RPE) $\geq$18, and peak HR $\geq$ 90% of age-predicted maximum

(220-age) (Fox 3rd et al., 1971). Respiratory gases were collected by the Vmax Encore

System (CareFusion Corp., San Diego, CA, USA) throughout the test, and $\dot{V}O_{2max}$ was

calculated as the highest oxygen consumption value averaged over 15 s before the end of

the test (Shi et al., 2018).

Repeated sprints cycling exercise

During the two experimental sessions, participants performed a repeated sprints set

consisting of 10 repetitions of 6 s maximal cycling sprints interspersed by 24 s resting. The

sprints were performed on a cycle ergometer (Monark Ergomedic 894E, Monark Exercise AB,

Vansbro, Sweden) connected to a laptop and controlled by software (Monark Anaerobic

Test Software, Monark Exercise AB, Vansbro, Sweden). After adjusting the seat height, each

participant sat upright on the cycle ergometer, and was instructed to keep the head as

steady as possible with the help of a neck cushion to minimise motion artefacts during NIRS

recordings. Before the repeated sprints, participants performed a 5-min warm-up, cycling at

a power output of 60 W (resistance, 1 kg; cadence, 60 rpm). During the sprints, participants

were instructed to use the same ready position, sitting upright and with one leg ready to

push powerfully against the pedal and maximally accelerate the cycling crank at the "go"

signal. Each participant was free to choose his leading leg in the first session and was asked

to use the same leg to initiate all following sprint repetitions. Five seconds into the next

sprint, participants moved into the ready position and awaited the verbal go command at

the end of a 3-s countdown. A weight equal to 6.5% body mass was applied to the flywheel

controlled by the Monark Anaerobic Test Software at the instant the pedalling cadence

reached 90 rpm. The controlling software recorded the mean power output for each sprint.

NIRS

A portable 2 x 4-channel continuous-wave NIRS system (Octamon, Artinis Medical Systems,

Einsteinweg, The Netherlands) was used to measure changes (Δ) in O_2Hb, HHb, and tHb

concentrations using two wavelengths at 750 and 850 nm. Data were acquired with the

OxySoft software (OxySoft, Artinis Medical Systems, Einsteinweg, The Netherlands) at a

frequency of 50 Hz with a differential path length factor of six. The optodes were attached

to a dark ambient light-protecting probe holder, tightly secured to the head by adjustable

headbands. The probe was placed over the forehead to scan the underlying prefrontal

cortex (four channels on each side). Care was taken to remove the hair under the optodes to

ensure optimal optical coupling between optodes and skin. The two light detectors were

aligned on Fp1 and Fp2 locations of the 10-20 system for the electroencephalography and

surrounded by four light-emitting optodes with an inter-optode distance of 35 mm,

providing a total of eight NIRS channels.

Impedance cardiography

Cardiac output was measured continuously during the sessions by signal morphology

impedance cardiography (PhysioFlow PF-05, Manatec biomedical, Paris, France). This device

measures cardiac output based on changes in thoracic impedance associated with the

ejection of blood by the left ventricle in each cardiac cycle, allowing the non-invasive

determination of stroke volume and cardiac output (Charloux et al., 2000). After skin

preparation to minimise electrical resistance, six Ag/AgCl electrodes (Hewlett Packard 40493

E) were placed on the chest wall along the xiphoid process and at the V1 and V6 precordial

locations, and at the base of the neck to record the thoracic impedance and

electrocardiographic signals. Resting blood pressure was measured by automatic

oscillometry to calibrate the cardiac impedance data acquisition. Stroke volume and cardiac

output were recorded for each cardiac cycle and measured continuously throughout the

trial.

Blood glucose and lactate

Blood glucose measurements were collected with a glucometer (ACCU−CHEK Performa, USA)

and the proper test strips (F. Hoffmann-La Roche AG, Basel, Switzerland). Blood lactate was

also measured using a handheld device and the appropriate test strips (Lactate Pro 2, AKRAY

Europe B.V., Amstelveen, the Netherlands). Both blood analytes were measured in duplicate

from capillary blood drawn from a lanceted fingertip at three time points: 1) at baseline,

soon after arrival to the laboratory; 2) immediately before starting the exercise protocol;

and 3) immediately after completion of the repeated sprints exercise. The two blood sample

measurements collected at each time point were averaged for analysis.

Procedures

Participants arrived at the laboratory between 8:00 and 9:00 am after a 12-hours fast. Soon

after arrival, participants ingested 300 ml of a drink containing 70 g of glucose (Cambridge

Isotope Laboratories, Cambridge, MA, USA) or a taste-matched placebo containing artificial

sweeteners (Truvia Calorie-Free Sweetener; Cargill, IL, USA). Afterwards, they rested sitting

for the next hour. Fifteen minutes to the end of the one-hour resting, participants were

fitted with the cardiac output, and NIRS instrumentations and the two devices were set up

for acquisition. The trial started with 10 minutes of seated resting, while wearing a cushion

around the neck to reduce head movement.

After the 10-min rest, each participant performed a battery of cognitive tests that took

approximately 15 minutes to complete (data not shown). Next, they mounted the cycle

ergometer and completed the 5-min warm-up followed by the 10 x 6-s repeated sprints.

After exercise, there were another 10 minutes resting followed by a second round of

cognitive testing (data not shown). Ratings of perceived exertion were obtained at the end

of the fifth and tenth sprint repetitions using the Borg's scale.

Data analysis

The NIRS data pre-processing was performed using the Homer2 toolbox (Huppert et al.,

2009) for Matlab (Matlab version 9.5.0, release R2018b, The Mathworks Inc., Natick,

Massachusetts, USA). First, light absorption data were converted into optical density and

haemoglobin concentrations using the modified Beer-Lambert law with a differential path

length factor of six. Next, all NIRS signals were low pass filtered at a cut-off frequency of 0.5

Hz to remove heartbeat-associated changes in O_2Hb, HHb and tHb. Filtering used a finite

impulse response fourth-order Butterworth filter, implemented in the forward and inverse

directions to avoid phase filtering artefacts (Huppert et al., 2009). After filtering, the whole

NIRS signal was epoched into the individual sprints, starting at minus 5 s and ending at 25 s

post the sprint start. Changes in O_2Hb, HHb and tHb were quantified using the median

change in the time intervals 0-15 s and 15-25 s, to measure the response during the sprints

and during the short time interval separating the sprints, respectively. The median was

chosen to quantify ΔO_2Hb, ΔHHb and ΔtHb because of its higher robustness against

potential biasing effects caused by motion artefacts and outliers. The time interval 0-15 s

was selected following a visual inspection of the transient ΔO_2Hb response accompanying

the performance of the sprints (Fig. 3). Because ΔO_2Hb, ΔHHb, and ΔtHb values were not

always normally distributed (Supporting information, Figs. S1-S3 and Table S1), they were

natural log-transformed for statistical analysis purpose.

Statistical analysis

The Shapiro-Wilk test was used for assessing the normal distribution of data. Repeated

measures ANOVA with complete factorial design (cerebral oximetry data: 2 trials x 8

channels x 10 sprint repetitions; power output and cardiovascular data: 2 trials x 10 sprint

repetitions) was used for testing responses to repeated sprints exercise. The Greenhouse-

Geiser correction was applied to within-subject factors violating the sphericity assumption

(Mauchly's test p-value < 0.05). In case of significant interaction effects or main effects, post

hoc tests were performed employing one-way ANOVA with Bonferroni's correction for

family-wise error rate. Significant main effects for repeated sprints were followed by

planned contrasts using polynomial fitting, assuming the repeated sprints as an evenly

separated quantitative variable. Although polynomial contrast analysis do not specifically

compare between two sprint repetitions, it offers relevant insight into the trend effect of

the repeated sprints on the response variables. In case of a significant linear contrast,

backward differences contrasts were computed (the contrast between two consecutive

sprint repetitions, including resting). Further contrasts between the first repeated sprint and

the following sprints were also calculated. One sample t-test was used for testing the

significance of post-exercise mean ΔO_2Hb, ΔHHb and ΔtHb against pre-exercise values

(since continuous NIRS measurements are relative, O_2Hb and HHb baseline concentrations

are set to zero). Correlation values were computed using the Pearson's coefficient. All

statistical tests were performed in RStudio (v. 1.3.1093, 2009-2020 RStudio, PBC) using

functions from Rstatix (v. 0.7.0) and R base (v. 4.0.3) packages. Unless otherwise stated, all

data are reported as mean $\pm$ standard deviation (SD). Significance was accepted at $p < 0.05$.

Results

The data from one participant were removed from the final analysis due to failure in

collecting the NIRS signals, so the final sample size was 10 participants. In one participant,

the NIRS signals recorded during three repeated sprints in the two trials were excluded from

analysis because of significant motion artefacts. The missing data (48 out of 1600 data

points) were replaced with the average from the same individual, channel, and remaining

sprints. In one participant (PLA trial), the mean power output in the two final repeated

sprints was not measured due to equipment failure. These missing values were replaced

with the last mean power output recorded.

Power output and RPE

Figure 1 illustrates the mean power output for each sprint and trial. Overall, the mean

power output was higher during the GLU trial than the PLA trial [GLU: 648 $\pm$ 183 W; PLA:

558 $\pm$ 161 W; $F_{(1, 9)}$ = 6.312, p = 0.033, η^2 = 0.098]. The higher power output in GLU was the

result of enhanced performance during later repeated sprints, in contrast with the PLA trial

where power output peaked in the first sprint and decreased thereafter [trial x sprint

repetition interaction effect: $F_{(2.79, 25.12)}$ = 12.314, p < 0.000, η^2 = 0.203]. One-way ANOVA,

testing the effect of trial at each sprint repetition, showed significant differences in mean

power output between GLU and PLA for sprint repetition number 1 (PLA higher than GLU), 7

and 10 (Bonferroni's corrected p < 0.05, Fig. 1). At the end of the fifth sprint, perceived

exertion was only moderate (GLU: 11.9 $\pm$ 2.1; PLA: 13.2 $\pm$ 1.9 units) but increased to

maximal or near-maximal values at the end of the repeated sprints set (GLU: 19.3 $\pm$ 2.1; PLA:

19.3 $\pm$ 0.5 units; main effect of sprint repetition, $F_{(1, 9)}$ = 232.66, p < 0.000, η^2 = 0.856). No

differences between trials or an interaction effect between trial and sprint repetition could

be found for RPE scores.

Blood glucose and lactate

Two-way ANOVA revealed a significant effect of time point [$F_{(2, 18)}$ = 13.143, p < 0.000, η^2 =

0.206] and a significant interaction between time point and trial for blood glucose

concentration [$F_{(2, 18)}$ = 9.666, p < 0.001, η^2 = 0.151]. At baseline, blood glucose

concentration was similar in the two trials (GLU: 5.7 $\pm$ 0.5 mmol·l^{-1}; PLA: 5.9 $\pm$ 0.6 mmol·l^{-1}; p

= 0.310), but at the beginning of exercise was significantly elevated with glucose ingestion

(GLU: 8.1 ± 1.7 mmol·l^{-1}; PLA: 6.1 ± 0.8 mmol·L^{-1}; p = 0.016). At the end of the repeated

sprints, blood glucose concentration was again similar in the two trials (GLU: 6.5 ± 1.6

mmol·l^{-1}; PLA: 5.9 ± 0.9 mmol·l^{-1}; p = 0.254).

Two-way ANOVA revealed a significant effect of time point [$F_{(1.14, 10.3)}$ = 605.698, p <0.000,

η^2 = 0.964] and a significant interaction between time point and trial for blood lactate

concentration [$F_{(2, 18)}$ = 11.193, p < 0.000, η^2 = 0.156]. At baseline, blood lactate

concentration was similar in the two trials (GLU: 1.7 ± 0.9 mmol·l^{-1}; PLA: 1.4 ± 0.4 mmol·l^{-1}; p

= 0.335), but increased after glucose ingestion and at the beginning of exercise it was higher

in GLU compared to PLA (GLU: 2.4 ± 0.8 mmol·l^{-1}; PLA: 1.6 ± 0.5 mmol·l^{-1}; p = 0.023).

Immediately after the repeated sprints, blood lactate was markedly elevated and

significantly higher in the PLA trial compared to the GLU trial (GLU: 10.8 ± 1.1 mmol·l^{-1}; PLA:

11.7 ± 1.4 mmol·l^{-1}; p = 0.047).

Heart rate, stroke volume, and cardiac output

Figure 2 depicts the heart rate, stroke volume and cardiac output responses to the repeated

sprints. Heart rate increased progressively across the repeated sprints set, rising from a

pooled average of 85 ± 4 beats·min^{-1} at rest to 110 ± 5 beats·min^{-1} during the first sprint,

further increasing to a peak value of 163 ± 5 beats·min^{-1} in the final sprint [main effect for

sprint repetition, excluding resting values: $F_{(3.45, 31.04)}$ = 347.947, p < 0.000, η^2 = 0.884]. No

differences in heart rate existed between GLU and PLA trials [$F_{(1, 9)}$ = 0.018, p = 0.897, η^2 <

0.000]. Also, no interaction effect between trial and sprint repetition could be found for

heart rate [$F_{(2.67, 24.03)}$ = 0.885, p = 0.453, η^2 = 0.023].

Stroke volume increased from 84.2 ± 5.8 ml at rest to 97.3 ± 8.4 ml during the first sprint,

but reached a plateau after the fourth sprint repetition [main effect for sprint repetition,

excluding resting values: $F_{(2.47, 22.25)} = 39.546$, $p < 0.000$, $\eta^2 = 0.380$]. No differences between

GLU and PLA [$F_{(1, 9)} = 0.195$, $p = 0.669$, $\eta^2 = 0.005$] or an interaction effect between trial and

sprint repetition [$F_{(2.14, 19.28)} = 1.199$, $p = 0.326$, $\eta^2 = 0.020$] could be found for stroke volume

during the repeated sprints.

Cardiac output increased during the repeated sprints with a curvilinear pattern, rising from a

resting cardiac output of 7.2 ± 0.7 l·min^{-1} to a cardiac output of 10.7 ± 1.0 l·min^{-1} in the first

sprint and 19.1 ± 1.1 l·min^{-1} at the end of the repeated sprints [main effect for sprint

repetition, excluding resting values: $F_{(2.59, 23.31)} = 214.561$, $p < 0.000$, $\eta^2 = 0.792$]. Cardiac

output was similar in the GLU and PLA trials [$F_{(1, 9)} = 0.280$, $p = 0.610$, $\eta^2 = 0.005$], and no

interaction effect between trial and sprint repetition was found for cardiac output [$F_{(1.93, 17.38)}$

$= 1.122$, $p < 0.346$, $\eta^2 = 0.025$].

In the time intervals between sprints, cardiac output remained elevated, with only a small

albeit significant decrease from its level during the sprints [overall mean $\pm$ SD during

sprinting, 16.2 ± 2.8 l·min^{-1}; in between sprints, 16.1 ± 2.8 l·min^{-1}; $F_{(1, 9)} = 6.084$, $p = 0.036$, η^2

$= 0.003$]. Polynomial contrasts revealed a significant linear and quadratic effect of sprint

repetition on heart rate, stroke volume and cardiac output responses. Several backward

differences contrasts were also significant (see Fig. 2 for details).

Brain oximetry

Table 2 presents the results for ΔO_2Hb, ΔHHb, ΔtHb during the repeated sprints and the

time interval between the sprint repetitions.

Oxyhaemoglobin

During the sprints, there was a rapid increase in O_2Hb that peaked near the end of the

sprints (Fig. 3; Supporting information, Fig. S4). As for cardiovascular parameters, ΔO_2Hb

across the sprints followed a curvilinear pattern. Therefore, three-way repeated measures

ANOVA found a significant main effect of sprint repetition on log-transformed O_2Hb

concentration response [$F_{(9, 81)}$ = 3.380, p = 0.001, η^2 = 0.074]. However, no significant effect

could be found for glucose ingestion [$F_{(1, 9)}$ = 0.930, p = 0.360, η^2 = 0.005] or NIRS channel

[$F_{(7, 63)}$ = 10.222, p = 0.979, η^2 = 0.002]. Polynomial fitting of ΔO_2Hb concentration values

showed a significant linear effect of sprint repetition on ΔO_2Hb without additional

improvement of fitting higher-order components. Further contrast analysis revealed a

significantly lower ΔO_2Hb in the first sprint compared to the fourth sprint and the next ones

(p < 0.05). No backward difference contrasts were found for ΔO_2Hb between two

consecutive sprints. After sprint cessation, O_2Hb concentration dropped to pre-sprint levels

or below (Fig. 3, Table 2). No significant differences between trials, channel, or sprint

repetitions could be found for ΔO_2Hb values in the time interval between sprints.

Deoxyhaemoglobin

Compared to ΔO_2Hb, ΔHHb responses to the repeated sprints were of a smaller magnitude

(Table 2, Fig. 3; Supporting information Fig. S4). No significant differences in ΔHHb were

found across the repeated sprints [$F_{(9,81)}$= 1.446, p = 0.182, η^2 = 0.01] or NIRS channels

[$F_{(7,63)}$= 1.531, p = 0.173, η^2 = 0.02]. Also, ΔHHb was similar in the two trials [$F_{(1, 9)}$= 0.476, p =

0.508, η^2 = 0.000] (Table 2). During the time interval separating the repeated sprints, HHb

returned towards pre-exercise levels, with no differences between trials [$F_{(1, 9)}$= 0.287, p =

0.605, $\eta^2 = 0.000$] or NIRS channel [$F_{(7,63)} = 1.162$, p = 0.337, $\eta^2 = 0.01$], but with a significant

main effect of sprint repetition [$F_{(9, 81)} = 2.152$, p = 0.034, $\eta^2 = 0.012$]. However, polynomial

contrasts found only marginal linear (p = 0.052) and quadratic (p = 0.057) effects of

repeated sprints on ΔHHb in the time interval between sprints.

Total haemoglobin

ΔtHb resembled ΔO_2Hb, with a marked increase during each sprint bout, followed by a fast

decline towards baseline immediately after the end of the sprint, without any effect of

glucose ingestion [$F_{(1, 9)} = 0.970$, p = 0.350, $\eta^2 = 0.007$] or NIRS channel [$F_{(7, 63)} = 0.403$, p =

0.897, $\eta^2 = 0.006$]. A significant interaction effect between trial and NIRS channel was found

for ΔtHb [$F_{(7, 63)} = 2.221$, p = 0.044, $\eta^2 = 0.009$]. However, when testing the difference

between GLU and PLA trials at each channel, no significant differences were found after

correction for multiple comparisons. Also, there was a significant difference in ΔtHb across

the repeated sprints [$F_{(9, 81)} = 2.796$, p = 0.007, $\eta^2 = 0.054$], with a significant linear effect (p =

0.008) and with smaller ΔtHb in the first sprint as compared to all the other sprint

repetitions (0.003 < p < 0.046) excepting to the third sprint (p = 0.061). Regarding backward

difference contrasts, only the difference between the second and first sprints was found

significant (p = 0.046). No differences between trials [$F_{(9, 81)} = 2.017$, p = 0.189, $\eta^2 = 0.002$],

NIRS channels [$F_{(7, 63)} = 1.016$, p = 0.429, $\eta^2 = 0.017$] or sprint repetitions [$F_{(9, 81)} = 0.866$, p =

0.560, $\eta^2 = 0.010$] were found for ΔtHb during the time interval between sprint repetitions.

We also compared the O_2Hb, HHb, and tHb concentrations at the onset of the warm-up, at

the end of exercise, and at 10-15 min post-exercise (see Fig. 3, top and middle panels).

Because of the small negative ΔO_2Hb after each sprint repetition, at the end of the repeated

sprints set O_2Hb concentration had decreased significantly relative to the time before the

warm-up (one sample t-test, GLU and PLA pooled together: $t(8)$ = -2.644; p = 0.029, n = 9).

This decrease in O_2Hb concentration at the end of the whole repeated sprints set was not

affected by glucose ingestion [GLU: -1.16 $\pm$ 4.13 μM; PLA: -3.11 $\pm$ 2.87 μM; $F_{(1,7)}$ = 2.453, p =

0.161, η^2 = 0.096, n = 9]. Contrary to O_2Hb, cerebral HHb concentration increased steadily

throughout the repeated sprints set and at the end of the exercise, it was significantly

elevated compared to pre-exercise (one sample t-test, GLU and PLA pooled together: $t(8)$ =

3.248, p = 0.011, n = 9), without any effect of glucose ingestion [GLU: 3.80 $\pm$ 5.95 μM; PLA:

6.44 $\pm$ 3.82 μM; $F_{(1,7)}$ = 1.541, p = 0.254, η^2 = 0.042, n = 9]. Due to the increase in HHb, tHb

at the end of the repeated sprints set was significantly elevated compared to pre-exercise

(one sample t-test, GLU and PLA pooled together: $t(8)$ = 3.119, p = 0.014, n = 9) and

irrespectively of glucose ingestion [GLU: 3.98 $\pm$ 5.60 μM; PLA: 5.75 $\pm$ 3.86 μM; $F_{(1,7)}$ = 0.670,

p = 0.440, η^2 = 0.014, n = 9]. After exercise, O_2Hb started to rise towards pre-exercise level.

The increase in O_2Hb during recovery was enhanced in the GLU trial [GLU: 2.54 $\pm$ 1.80 μM;

PLA: 0.95 $\pm$ 2.32 μM; $F_{(1,7)}$ = 11.263, p = 0.012, η^2 = 0.140, n = 9]. As a result, post-exercise

O_2Hb was above pre-exercise values in the GLU trial (one sample t-test, $t(8)$ = 8.099, p <

0.000, n = 9) but not in the PLA trial (one sample t-test, $t(8)$ = 2.018, p = 0.08, n = 8). At 10-

15 min post-exercise, HHb remained similarly elevated in both trials [GLU: 3.42 $\pm$ 4.02 μM;

PLA: 3.55 $\pm$ 3.15 μM; $F_{(1,7)}$ = 0.023, p = 0.884, η^2 < 0.000, n = 9] compared to pre-exercise

values (one sample t-test, GLU and PLA pooled together: $t(8)$ = 4.557, p = 0.001, n = 9).

Following the changes in HHb and O_2Hb, tHb concentration also rose after the repeated

sprint exercise in both trials [Glu: 3.29 $\pm$ 4.07 μM; Pla: 3.12 $\pm$ 3.31 μM; $F_{(1,7)}$ = 0.050, p =

0.829, η^2 < 0.000, n = 9] and at 10-15 min post-exercise, it was above pre-exercise level (one

sample t-test, GLU and PLA pooled together: $t(8)$ = 3.882, p = 0.005, n = 9).

Cardiac output and ΔO_2Hb, ΔHHb and ΔtHb relationship

Figure 4 presents the scatter plots with the relationship between cardiac output, power

output, and cerebral haemoglobin concentrations (see also Supporting information, Fig. S5).

During the sprint exercise, ΔO_2Hb and ΔtHb were positively correlated with cardiac output

in both GLU (CO: ΔO_2Hb, R = 0.85, p = 0.0019; CO: ΔtHb, R = 0.86, p = 0.0013) and PLA trials

(CO: ΔO_2Hb, R = 0.87, p = 0.0012; CO: ΔtHb, R = 0.85, p = 0.0016). No significant correlation

was found between cardiac output and ΔHHb during the repeated sprints. Also, no

correlation was found between cardiac output and ΔO_2Hb, ΔHHb and ΔtHb during the time

interval between the sprints. During sprints, ΔO_2Hb was negatively correlated with power

output in the PLA trial. In the GLU trial, power output was negatively correlated with ΔO_2Hb

values during the time interval between the sprints.

Discussion

In this study, we sought to describe the time course of cerebral O_2Hb, HHb and tHb

response to the performance of a series of short, repeated sprints and assess the

relationship between this response and cardiac output. Additionally, we explored the

modulating effect of acute hyperglycaemia on O_2Hb, HHb and tHb changes in response to

the repeated sprint exercise. We showed that each of the short, repeated sprints produced

a rapid and substantial increase in O_2Hb and, to a lesser extent HHb, resulting in a transient

elevation of cerebral blood volume (i.e., increased tHb) and cerebral oxygenation. In the

time interval between the repeated sprints, O_2Hb and HHb returned toward or below pre-

exercise levels also in a short time. The magnitude of ΔO_2Hb and ΔtHb followed a curvilinear

pattern across the repeated sprints set that resembled the heart rate and cardiac output

responses to the repeated sprint exercise.

The short sprints in this study elicited an approximately ten-fold increase in O_2Hb, compared

to the pulsatile peak increase due to the heartbeat at rest (~0.5 μM). Increased cardiac

output and cerebral perfusion pressure, the latter due to elevation of arterial blood

pressure, are two credible reasons for this transient increase in O_2Hb and HHb during each

short sprint (Cifford et al., 1994; Curtelin et al., 2018; Pott et al., 1997). Although blood

pressure was not recorded in this study, an increase in mean blood pressure is expected to

occur during all-out sprint exercise, based on previous studies revealing that both heavy-

intensity dynamic (e.g., rowing exercise) and resistance (e.g., leg-press exercise) types of

exercise cause a rapid increase in diastolic and systolic blood pressures (Cifford et al., 1994;

Curtelin et al., 2018; Edwards et al., 2002; Perry & Lucas, 2021). While enhanced central

drive and activation of the metaboreflex cannot be discarded as mechanisms contributing to

the sprint-induced elevation of blood pressure (Gandevia & Hobbs, 1990), the immediate

and transient increase in O_2Hb and HHb during the short sprint exercise suggests a role for

mechanical and haemodynamic factors associated with the powerful contraction of the leg

and trunk muscles, resulting in brief Valsalva-like manoeuvres and in synchronous elevation

of arterial blood pressure (Perry & Lucas, 2021; Pott et al., 1997; Sejersen et al., 2021; Zhang

et al., 2004). Although more often associated with heavy static and dynamic resistance

exercise (Perry & Lucas, 2021; Pott et al., 2003), Valsalva-like manoeuvres are also

characteristically observed during dynamic exercise, such as during the catch phase of

rowing (Pott et al., 1997; Sejersen et al., 2021), where there is a cyclical increase in MCAv

synchronous with the elevation of intra-abdominal pressure, central venous pressure, and

catch force (Pott et al., 1997). Similarly, the onset of bilateral static leg extension

concomitantly rises mean arterial blood pressure, MCAv and cerebral O_2Hb concentration

with or without a superimposed Valsalva strain (Pott et al., 2003). Whether a similar

Valsalva-like manoeuver occurs during cycling sprints is unclear. However, participants in

this experiment cycled against a considerable load (i.e., 6.5% body weight; mean load, 5.8

kg), maintaining high levels of power output (pooled average ~ 600 W) during the entire

sprint duration. This power output level is close to that reported during 10 maximal leg

press resistance exercise in a fitter population (Gorostiaga et al., 2012), an exercise type

that has been shown to increase mean arterial pressure, MCA*v*, and CBF (Perry & Lucas,

2021). Also, the simultaneous contraction of the leg and abdominal muscles during cycling

sprint might have produced a transient increase in cardiac output, due to the combined

action of the muscle and respiratory pumps (Aliverti et al., 2009).

Cardiac output directly influences CBF and cerebral oxygenation independently from

changes in arterial blood pressure (Castle-Kirszbaum et al., 2022; Lie et al., 2021; Ogoh,

Brothers, et al., 2005). In our study, cardiac output values during the sprints were

moderately and positively correlated with ΔO_2Hb and ΔtHb, which suggests that cardiac

output might contribute to changes in CBF and cerebral oxygenation during the repeated

sprints. Cardiac output progressively increased over the repeated sprints set, which was akin

to the transient ΔO_2Hb response to each sprint exercise, thus suggesting that cardiac output

was at least partly driving the rise in O_2Hb during the sprints. The ability of cardiac output in

raising CBF independently from cerebral perfusion pressure is controversial. During static

leg exercise, changes in MCAv seems to develop in divergence with cardiac output (Pott et

al., 2003), but a direct relationship between cardiac output and MCAv has been reported

during rest and moderate intensity cycling exercise (Ogoh, Brothers, et al., 2005). However,

an enhanced blood pressor response with increasing number of sprint repetitions, as a

result of enhanced central drive and exercise pressor reflex (Gandevia & Hobbs, 1990;

Stebbins et al., 2002) or stronger Valsalva manoeuver as a response to the developing

fatigue and increased feelings of exertion with increasing number of sprint repetitions

(Perry et al., 2014), could have also contributed to the increased $\Delta O_2 Hb$ and ΔtHb across the

repeated sprints set, irrespective of cardiac output. Moreover, and in spite of its relationship

with $O_2 Hb$ and tHb during the sprints, cardiac output seems to have exerted little influence

on cerebral haemoglobin concentration levels in the intervals between the repeated sprints.

After each sprint, there was a clear deviation between cardiac output and cerebral

haemoglobin concentration, with $O_2 Hb$ and tHb rapidly returning to baseline despite cardiac

output remaining elevated. Therefore, a high cardiac output seems unsufficient to raise

$O_2 Hb$ and tHb without additional mechanisms that are acting during the sprint exertion. The

simplest explanation for the fast decrease in cerebral $O_2 Hb$ and tHb concentrations with the

end of the sprint is an also sudden decrease in mean arterial blood pressure upon cessation

of the heavy cycling exercise (Curtelin et al., 2018; Edwards et al., 2002). Curtelin et al.

(Curtelin et al., 2018) reported a drop in mean blood pressure immediately after the end of

a Wingate test, which was approximately three times larger than its increase during the

effort. Moreover, this decrease in mean blood pressure was accompanied by a significant

decline in MCAv, which lasted for approximately 40 s before returning to pre-exercise levels

(Curtelin et al., 2018). However, a decrease in CBF at the end of exercise might occur

independently from changes in arterial blood pressure. Pott et al. (Pott et al., 1997)

reported a continuous decrease in MCAv after each rowing's catch movement in spite of

stable mean blood pressure, which these authors suggest could have been caused by the

delayed cerebral autoregulation response. A similar event could have taken place during

the repeated sprints, considering the match between the repeated sprints duration and the

phase delay of cerebral autoregulation (Fantini et al., 2016).

The performance of the repeated sprints exercise was accompanied with decreased cerebral

O_2Hb and increased in HHb, although with sizeable interindividual variation (Fig 3). The rise

in HHb overcame the decrease in O_2Hb, hence cerebral tHb was also increased at the end of

the repeated sprints exercise. These alterations in cerebral oxygenation partially agree with

MCAv data recorded during the Wingate test, revealing decreased CBF and cerebral

oxygenation levels caused by augmented cerebral vascular resistance at later sprint stages

(Curtelin et al., 2018). A similar response is observed during heavy resistance exercise, with

cerebrovascular resistance increasing during exercise but lowering rapidly once the

muscular activity stops (Edwards et al., 2002). Our data extends these observations,

showing similarly restrained cerebral blood flow and cerebral oxygen delivery during short

cycling sprints, even when perceived exertion is only at moderate levels. Dynamic cerebral

autoregulation is a primary mechanism for regulating cerebrovascular resistance. The effect

of exercise on this mechanism is controversial, with studies indicating decreased efficacy of

dynamic autoregulation during exhaustive aerobic exercise (Ogoh, Dalsgaard, et al., 2005).

In contrast, other studies report unchanged or even enhanced cerebral autoregulation

during aerobic exercise (Brys et al., 2003). The protracted CBF recovery from hypotension

after heavy aerobic exercise (Ogoh et al., 2007) and sprinting (Curtelin et al., 2018) suggests

a diminished cerebral autoregulation efficacy, possibly combined with a reduced gain of the

arterial baroreflex (Ogoh et al., 2007). Our study cannot address the question of whether

performing short sprints affects cerebral autoregulation, but the rapid decrease in O_2Hb at

the end of the sprints when cardiac output was elevated suggests normal cerebral

autoregulation during this type of exercise. Future studies may test the effect of different

sprint/recovery cycle durations on cerebral haemoglobin responses. Also, lowered arterial

and brain CO_2 levels and sympathetic activity related to enhanced central drive or activation

of muscle metaboreceptors could have also contributed to the lowered oxygen delivery

during the repeated sprints (Curtelin et al., 2018). Importantly, a decline in O_2Hb during

repeated sprints contrasts with the increase in cerebral oxygenation during lower body

resistance exercise (Cherouveim et al., 2022; Zafeiridis et al., 2022). Since decreased brain

oxygen saturation is observed in other sprint studies (Curtelin et al., 2018), we may

conclude that the extreme intensity of sprint exercise and the recruitment of a large muscle

mass reduce cerebral blood flow and lowers cerebral oxygenation. The cessation of the

repeated sprints exercise was accompanied by a cerebral reactive hyperaemic response,

with a steep increase in O_2Hb within minutes following exercise (Fig. 3). This strengthens the

claim of inadequate cerebral oxygen delivery during the repeated sprints exercise.

In this experiment, we exploratory investigated the role of glucose ingestion and acute

hyperglycaemia on the response of cerebral haemoglobin to sprint exercise. Although the

brain almost exclusively relies on glucose for its metabolism and brain's glucose uptake

increases during exercise, hyperglycaemia has been shown to decrease the cerebral

metabolic rate of oxygen (Ishibashi et al., 2016; Shemesh et al., 2019) and brain connectivity

(Ishibashi et al., 2018) in healthy young participants. Acute and chronic hyperglycaemia also

decreases CBF (Duckrow et al., 1985; Shemesh et al., 2019). In our experiment, glucose

ingestion did not alter O_2Hb and HHb responses to the repeated sprints exercise, although

improving performance. However, reactive hyperaemia was significantly enhanced with

glucose ingestion, so that O_2Hb concentration increased faster and reached higher levels in

the post-exercise period with glucose ingestion. Whether post-exercise hyperaemia was

related to any baseline changes in CBF or cerebral blood volume caused by glucose ingestion

cannot be ascertained by our data and warrants further investigation.

Study limitations

The major limitation in this study is the possible confounding effect of extracerebral (scalp

and skull) haemodynamics. Since the emitted NIRS light traverses extracerebral tissues and

the cerebral cortex, changes in blood volume and flow in superficial tissues will inevitably

contaminate the NIRS measurements. The design of our NIRS probe, with rigid circular

optodes holders firmly secured to exert pressure onto the forehead skin underneath the

optodes, helps to minimise changes in skin blood flow and their impact on NIRS recordings

(Baker et al., 2015). Other procedures employ short separation channels to record the

contaminating signal from superficial tissues and use these signals to regress out the

influence of superficial tissue haemodynamics on the NIRS signals. However, our NIRS probe

did not allow recording from short separation channels and therefore the influence of

extracerebral tissues on the measured haemoglobin concentrations could not be

ascertained nor removed. The exact impact of exercise on extracerebral haemodynamics is

unknown. Facial skin blood flow and vascular conductance have been shown to increase

with dynamic exercise intensity without a clear plateauing (Hayashi et al., 2020), whilst

ocular circulation is similar to cerebral circulation, decreasing from elevated values to

baseline in response to exhaustive dynamic exercise (Ikemura & Hayashi, 2012). These

findings suggest that our oximetry data during the repeated sprints exercise mainly

originate from cerebral circulation. Future studies may assess the contribution of forehead

skin to changes in haemoglobin concentration in the frontal region of the cerebral cortex

during repeated sprints.

Conclusions

Short repeated cycling sprint exercise elicits a transient increase in O_2Hb, HHb and tHb. A

positive relationship exists between changes in O_2Hb and cardiac output during the sprint

exercise but not during the time interval separating the sprints. Despite its transient

increases, O_2Hb declined throughout the repeated sprints set. In contrast, HHb increased,

resulting in a progressive decrease in cerebral oxygen saturation as the number of sprint

repetitions increase, indicating insufficient brain oxygen delivery during short repeated

sprints exercise. Glucose ingestion did not alter O_2Hb, HHb or tHb responses to the repeated

sprint exercise but improved sprint performance and was associated with faster O_2Hb

increase during recovery.

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Conflicts of interests

The authors report no conflict of interests.

Author contributions

P.A.S. and H.M. conceived the study and were responsible for collecting, analysing and

interpreting the data and for writing the original draft. W.Z., W.L. and F.R. helped

conducting the experiments and collecting and analysing the data. X.Z. assisted in acquiring

and analysing NIRS data. Z.Y. and Z.K. co-supervised and conceived the study and assisted

with writing and revising the manuscript.

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Table 1: Participants characteristics. Data are presented as mean $\pm$ standard deviation; n = 11.

Age (years)	Height (cm)	Weight (kg)	BMI (kg·m^{-2})	% Body fat (%)	$\dot{V}O_{2peak}$ (ml·kg^{-1}·min^{-1})	HR$_{peak}$ (beats·min^{-1})	$\dot{W}_{peak}$ (W)
25 $\pm$ 3	174 $\pm$ 7	89 $\pm$ 11	29 $\pm$ 3	30 $\pm$ 5	32 $\pm$ 2	172 $\pm$ 4	132 $\pm$ 12

839   BMI, body mass index; $\dot{V}O_{2peak}$, peak value for the rate of oxygen consumption during the incremental maximal exercise test; HR$_{peak}$, peak value
840   for heart rate during the incremental maximal exercise test; $\dot{W}_{peak}$, peak value for power output during the incremental maximal exercise test.

842   Table 2: Mean $\pm$ SD values for oxyhaemoglobin, deoxyhaemoglobin, and total haemoglobin concentration changes during the repeated sprints;

843   n = 10.

Sprint repetition	Trial	$\Delta O_2Hb_{0-15\ sec}$ μM	$\Delta O_2Hb_{15-25\ sec}$ μM	$\Delta HHb_{0-15\ sec}$ μM	$\Delta HHb_{15-25\ sec}$ μM	$\Delta tHb_{0-15\ sec}$ μM	$\Delta tHb_{15-25\ sec}$ μM
1st	Placebo	1.81 $\pm$ 1.69	-0.18 $\pm$ 1.82	0.02 $\pm$ 0.39	-0.25 $\pm$ 0.66	1.83 $\pm$ 1.84	-0.44 $\pm$ 2.06
	Glucose	1.68 $\pm$ 1.00	0.30 $\pm$ 2.49	-0.11 $\pm$ 0.39	-0.35 $\pm$ 0.52	1.51 $\pm$ 1.96	-0.03 $\pm$ 2.42
	Mean $\pm$ SD	1.75 $\pm$ 1.84	0.06 $\pm$ 2.19	-0.04 $\pm$ 0.40	-0.30 $\pm$ 0.59	1.67 $\pm$ 1.90	-0.24 $\pm$ 2.25
2nd	Placebo	2.75 $\pm$ 1.33	-0.61 $\pm$ 1.56	0.25 $\pm$ 0.54	0.01 $\pm$ 0.49	3.01 $\pm$ 1.51	-0.62 $\pm$ 1.36
	Glucose	1.99 $\pm$ 1.82	-1.04 $\pm$ 1.42	0.16 $\pm$ 0.33	0.14 $\pm$ 0.43	2.16 $\pm$ 1.20	-0.88 $\pm$ 1.47
	Mean $\pm$ SD	2.37 $\pm$ 1.64	-0.82 $\pm$ 1.31	0.21 $\pm$ 0.45	0.08 $\pm$ 0.46	**2.59 $\pm$ 1.81**[a, b]	-0.75 $\pm$ 1.42
3rd	Placebo	2.61 $\pm$ 1.52	-0.38 $\pm$ 1.40	-0.01 $\pm$ 1.18	-0.22 $\pm$ 1.25	2.67 $\pm$ 1.61	-0.59 $\pm$ 2.01
	Glucose	2.24 $\pm$ 1.71	-0.55 $\pm$ 0.99	0.02 $\pm$ 0.29	-0.07 $\pm$ 0.43	2.30 $\pm$ 1.76	-0.60 $\pm$ 1.08
	Mean $\pm$ SD	2.42 $\pm$ 1.62	-0.47 $\pm$ 1.21	0.00 $\pm$ 0.85	-0.15 $\pm$ 0.94	2.48 $\pm$ 1.69	-0.60 $\pm$ 1.61
4th	Placebo	3.05 $\pm$ 1.71	-0.62 $\pm$ 1.43	-0.04 $\pm$ 0.82	-0.41 $\pm$ 0.93	3.11 $\pm$ 2.03	-1.04 $\pm$ 2.14

	Glucose	2.67 ± 1.39	-0.51 ± 1.26	0.01 ± 0.48	-0.16 ± 0.46	2.77 ± 1.57	-0.68 ± 1.45
	Mean $\pm$ SD	$\mathbf{2.86 \pm 1.56}$[a]	-0.57 ± 1.34	-0.02 ± 0.67	-0.28 ± 0.74	$\mathbf{2.94 \pm 1.82}$[a]	-0.86 ± 1.83
5th	Placebo	3.08 ± 1.95	-0.59 ± 0.67	0.10 ± 0.66	-0.16 ± 0.43	3.20 ± 2.22	-0.72 ± 0.82
	Glucose	3.17 ± 1.70	-0.24 ± 1.26	-0.05 ± 0.52	-0.19 ± 0.81	3.16 ± 1.60	-0.41 ± 1.79
	Mean $\pm$ SD	$\mathbf{3.12 \pm 1.83}$[a]	-0.42 ± 1.02	0.02 ± 0.60	-0.18 ± 0.64	$\mathbf{3.18 \pm 1.93}$[a]	-0.57 ± 1.49
6th	Placebo	3.18 ± 1.66	-0.17 ± 1.08	0.25 ± 0.73	0.00 ± 0.83	3.44 ± 2.00	-0.17 ± 1.70
	Glucose	2.88 ± 1.97	-0.59 ± 1.11	-0.04 ± 0.51	-0.12 ± 0.52	2.93 ± 2.11	-0.73 ± 1.39
	Mean $\pm$ SD	$\mathbf{3.03 \pm 1.83}$[a]	-0.38 ± 1.11	0.10 ± 0.64	-0.06 ± 0.69	$\mathbf{3.19 \pm 2.07}$[a]	-0.45 ± 1.58
7th	Placebo	2.75 ± 1.52	-0.47 ± 1.25	0.15 ± 0.77	-0.28 ± 0.70	2.94 ± 1.87	-0.74 ± 1.45
	Glucose	2.37 ± 1.25	-0.68 ± 1.02	0.07 ± 0.41	-0.12 ± 0.36	2.49 ± 1.49	-0.80 ± 1.16
	Mean $\pm$ SD	$\mathbf{2.56 \pm 1.34}$[a]	-0.57 ± 1.14	0.11 ± 0.62	-0.20 ± 0.56	$\mathbf{2.71 \pm 1.70}$[a]	-0.77 ± 1.31
8th	Placebo	3.03 ± 2.78	-0.60 ± 1.49	0.40 ± 1.02	-0.07 ± 0.92	3.47 ± 3.27	-0.66 ± 1.24
	Glucose	3.15 ± 2.34	-0.07 ± 1.10	0.09 ± 0.44	-0.15 ± 0.52	3.26 ± 2.45	-0.21 ± 0.93
	Mean $\pm$ SD	$\mathbf{3.09 \pm 2.56}$[a]	-0.33 ± 1.33	0.25 ± 0.80	-0.11 ± 0.75	$\mathbf{3.36 \pm 2.88}$[a]	-0.44 ± 1.12

		$\Delta O_2Hb_{0-15\,sec}$	$\Delta O_2Hb_{15-25\,sec}$	$\Delta HHb_{0-15\,sec}$	$\Delta HHb_{15-25\,sec}$	$\Delta tHb_{0-15\,sec}$	$\Delta tHb_{15-25\,sec}$
9th	Placebo	3.23 ± 2.70	-0.81 ± 1.33	0.02 ± 1.08	-0.54 ± 1.14	3.28 ± 3.15	-1.37 ± 2.11
	Glucose	2.72 ± 1.42	-0.26 ± 1.01	-0.04 ± 0.45	-0.35 ± 0.57	2.69 ± 1.55	-0.59 ± 1.30
	Mean ± SD	**2.98 ± 2.17**[a]	-0.54 ± 1.21	-0.01 ± 0.82	-0.44 ± 0.90	**2.98 ± 2.49**[a]	-0.98 ± 1.79
10th	Placebo	3.40 ± 3.01	-0.36 ± 1.46	0.10 ± 0.82	-0.29 ± 0.68	3.57 ± 3.56	-0.60 ± 1.70
	Glucose	3.50 ± 1.80	-0.35 ± 1.44	-0.22 ± 0.92	-0.58 ± 1.77	3.35 ± 1.78	-0.92 ± 2.22
	Mean ± SD	**3.45 ± 2.47**[a]	-0.35 ± 1.44	-0.06 ± 0.88	-0.43 ± 1.35	**3.46 ± 2.81**[a]	-0.76 ± 1.98
Overall mean ± SD	Placebo	2.89 ± 2.10	-0.48 ± 1.35	0.12 ± 0.84	-0.22 ± 0.85	3.05 ± 2.44	-0.70 ± 1.73
	Glucose	2.64 ± 1.84	-0.40 ± 1.41	-0.01 ± 0.51	-0.19 ± 0.77	2.66 ± 1.92	-0.59 ± 1.60

$\Delta O_2Hb_{0-15\,sec}$, median change in oxyhaemoglobin concentration in the time interval $0-15$ s (sprint); $\Delta O_2Hb_{15-25\,sec}$, median change in
oxyhaemoglobin concentration in the time interval $15-25$ s (recovery); $\Delta HHb_{0-15\,sec}$, median change in deoxyhaemoglobin concentration in the
time interval $0-15$ s (sprint); $\Delta HHb_{15-25\,sec}$, median change in deoxyhaemoglobin concentration in the time interval $15-25$ s (recovery); $\Delta tHb_{0-15\,sec}$
median change in total haemoglobin concentration in the time interval $0-15$ s (sprint); $\Delta tHb_{15-25\,sec}$, median change in total haemoglobin
concentration in the time interval $15-25$ s (recovery). Positive and negative values indicate increase and decrease in haemoglobin
concentrations, respectively, from the time immediately before the onset of the respective sprint repetition (baseline value = 0). Mean ± SD is
the average and standard deviation of values from GLU and PLA trials within each sprint. Overall mean ± SD is the average and standard
deviation for all values in the respective trial. [a] Significantly different from the first sprint, $p < 0.05$; [b] significantly different from the
immediately preceding sprint, $p < 0.05$.

Figure 1

Figure 1: Mean power output (mean ± SD) during each repeated sprint for GLU (red line)

and PLA (blue line) trials (left panel). Pooled mean power output (mean ± SD) for GLU (red

bar) and PLA (blue bar) trials (right panel). Data is mean ± SD; ns, non-significant, n = 10.

Figure 2

Figure 2: Heart rate, stroke volume and cardiac output (mean ± SD) at rest and during each repeated sprint for GLU (red lines) and PLA (blue lines) trials. The insert is the output of the two-way repeated measures ANOVA for the significant main effect of sprint repetition, excluding the resting values. P-values are from backward difference contrasts (contrast between one sprint repetition and the one immediately before, including the first sprint and resting values); n = 10.

869   Figure 3

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Figure 3: Changes in O₂Hb, HHb and tHb during the repeated sprints exercise. Top and

middle graphs depict changes in the concentration of O₂Hb (red line), HHb (blue line) and

tHb (green line) recorded in two participants. The records start immediately before the

warm-up. The transient increase in O₂Hb, HHb, and tHb during each sprint (black dots) is

clearly seen in both participants. In the top graph, there was a substantial decrease in O₂Hb

concentration and increase in HHb over the repeated sprints exercise and a return of both

O₂Hb and HHb toward pre-exercise values during recovery. The participant in the middle

graph had lesser changes in O₂Hb and HHb concentration during exercise but substantial

post-exercise cerebral hyperaemia. The bottom panel presents the overall average for

ΔO₂Hb and ΔHHb during the repeated sprints, showing the rapid increase in cerebral

haemoglobin concentration during the sprint and its fast decrease soon after the end of the

sprint. Each tracing is the mean of 10 participants, 10 sprints and 8 channels. The shadowed

areas represent the standard error of the mean; n = 10.

Figure 4

Figure 4: Scatter plots depicting the relationship between ΔO_2Hb (upper left graph), ΔHHb (upper right graph), and ΔtHb (lower left graph) with cardiac output and between ΔO_2Hb and power output (lower right graph) during the sprints (solid lines) and during the time interval between sprints (dotted lines) in GLU (red lines and red circles) and PLA (blue lines and blue triangles) trials. The Pearson's R coefficients and respective p-values are presented on the top of the graphs for values during the sprint (left column) and the time interval between the sprints (right column) for GLU (red font) and PLA (blue font) trials. During the sprint, a significant correlation was found between cardiac output and ΔO_2Hb and ΔtHb. No significant correlation was found between cardiac output and ΔHHb and cardiac output and

897   ΔO_2Hb and ΔtHb during the time interval between sprints. Mean power output was

898   negatively correlated with ΔO_2Hb during the sprints in PLA trial, and negatively correlated

899   with ΔO_2Hb in the time interval between sprints in the GLU trial.