A high-impact *COL6A3* mutation alters the response of chondrocytes in neo-cartilage

organoids to hyper-physiologic mechanical loading

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Abstract

Dysregulation of mechano-transduction via chondrocyte pericellular matrix (PCM) has been

shown to induce osteoarthritis (OA), a highly prevalent degenerative disease of joint tissues. By

performing exome sequencing in symptomatic OA patients, a high impact mutation in *COL6A3*

encoding one of the monomeric sub-unit-3 of collagen type VI (COLVI) was identified. COLVI

is an essential and specific protein functioning in the PCM. To study the downstream effects of

the mutation in interaction with hyper-physiologic mechanical loading conditions, genetically

COL6A3-edited human induced pluripotent stem cells (hiPSCs) were employed in our established

in-vitro cartilage organoid model. We showed mutated COLVI had significant lower binding to

fibronectin (FN) and provoked an osteoarthritic chondrocyte state. Moreover, the *COL6A3*

mutation abolished the initial stress responses of chondrocytes to hyper-physiological mechanical

loading conditions. Together, the established sustainable cartilage organoid model provides unique

opportunities to study the transduction of mechanical cues to chondrocytes and explore ways to

counteract effects.Acquired insights could guide effective treatment development for OA.

Introduction

Osteoarthritis (OA) is a complex, multifactorial disease revolving around the interplay between

genetic and environmental risk factors. In particular, biomechanical cues play a critical role in not

only joint health but also drive the onset and progression of disease (*1*). Indeed, physiologic levels

of mechanical loading by virtue of physical exercise can slow down OA disease progression (*2,*

3). In contrast, hyper-physiological loading, as seen with post-traumatic injuries such as articular

fracture, meniscal tear, or rupture of the anterior cruciate ligament, concomitant with altered joint

kinematics, is a major risk factor for the onset and progression of OA (*4*). Both physiological and

hyper-physiological loading results in alterations in the structural composition of the cartilage

extracellular matrix (*1*). These findings suggest that the balance of chondrocyte anabolic and

catabolic processes for the maintenance of cartilage is tightly regulated by biomechanical cues.

Chondrocytes reside in a pericellular matrix (PCM), which modulates the transduction of

mechanical cues from the extracellular matrix (ECM) towards the chondrocyte. The PCM for that

matter contains specific proteins such as collagen 6 (COLVI) and fibronectin (FN) (*5*). In

particular, collagen 6 (COLVI) is involved in regulating the mechanical properties of the PCM as

well as calcium signaling in response to mechanical stress (*5-7*). Knock-out of a COLVI sub-unit,

COL6A1, in a murine model induces an osteoarthritic phenotype through dysregulation of

mechano-transduction (*6, 8*). While loss of COLVI in humans is characterized by joint

contractures, hyperlaxity, and myopathy resulting in an inability to ambulate (*9*), the effect of

aberrant COLVI function on chondrogenesis and mechano-transduction remains unclear.

Here we report the identification of a *COL6A3* missense mutation through exome sequencing of

affected sibling pairs with generalized OA. *COL6A3,* coding for one of the monomeric sub-units

of COLVI (*10*) that resides in (*6*) and interacts with other PCM proteins (*11, 12*), is likely involved

in the regulation of cartilage structural composition and mechanical properties. We hypothesized

that the identified *COL6A3* mutation would perturb cartilage mechano-transduction in response to

hyper-physiologic loading, thereby contributing to OA pathogenesis. Recently, OA disease

modeling platforms utilizing human induced pluripotent stem cells (hiPSCs) have been used to

facilitate the interrogation of these pathogenic variants (*13*). To gain an understanding of the role

of COLVI in cartilage, we studied this mutation in an *in vitro* model of OA using hiPSC-derived

cartilage. We employed genetically *COL6A3*-edited hiPSCs to an established *in vitro* cartilage

organoid model, and these neo-cartilage organoids were exposed to hyper-physiological

mechanical loading conditions. The effects of the mutation on COLVI's interaction with other

PCM proteins was studied. To study the downstream effects of this mutation in response to hyper-

physiologic mechanical loading conditions, we characterized downstream molecular pathways

based on transcriptome wide profiles. Understanding the role of COLVI in the regulation of

mechanical stress will provide insight into etiology of OA and guide the development of effective

treatment strategies for OA.

Results

Whole exome-sequencing was applied to a Caucasian sib pair of Dutch ancestry at age of 61

affected predominantly with symptomatic OA at multiple sites (GARP study) (*14*). This resulted

in the detection of 81,416 genetic variants, after which a prioritization schema was followed to

identify pathogenic variants as previously described (*15*). In short, first, we selected novel variants

in in-house whole genome sequencing projects (N=222) and the BBMRI-Genome of the

Netherlands project (GoNL, N=473) (*15*). And second, damaging missense variants were selected

based on the prediction of sorting intolerant from tolerant (SIFT). This prioritization generated a

dataset of 38 novel coding variants that were predicted to have a functional impact on the protein

(table S1). And third, these 38 novel coding variants were then further prioritized based on their

expression patterns in disease-relevant tissue by means of *in silico* analysis of 58 paired lesioned

and preserved samples, resulting in two genes that are highly expressed in cartilage and

differentially expressed between lesioned and preserved cartilage and bone; *MTHFR* (c.1667C>T,

p.Pro597Leu; cartilage: FC=0.84, FDR=0.04, bone: not detected) and *COL6A3* (c.4510C>T,

p.Arg1504Trp; cartilage: FC=1.75, FDR=2.25×10^{-5}, bone: FC=1.69, FDR=0.042) (*16*). *MTHFR*

encodes for methylenetetrahydrofolate reductase, which is involved in folate metabolism (*17*).

COL6A3 encodes for collagen VI subunit A3, which together with collagen VI subunit A1 and A2

forms a triple helical COLVI, a primary component of the cartilage PCM, and interacts with other

proteins such as fibronectin and hyaluronan (*11, 12, 18*). The identified COL6A3 mutation is

located in the N-terminal VWA domains that are known to protrude away from the triple helical

structure. The *COL6A3* mutation was selected based on COLVI's role in regulating transduction

of mechanical cues in cartilage towards chondrocytes (*6*). To gain an understanding of aberrant

COLVI function in cartilage, we selected this high-impact mutation for studying its effects in 3D

in-*vitro* models of cartilage, and in interaction with hyper-physiological mechanical loading

conditions.

Introducing the mutation in hiPSCs

To investigate the effects of the aberrant COLVI on COLVI-mediated matrix deposition and

molecular pathways, a gene-edited human induced pluripotent stem cell (hiPSC)-derived neo-

cartilage organoid model was generated. We employed CRISPR-Cas9 single-stranded

oligonucleotide-mediated homology-directed repair in hiPSCs to attain biallelic modification of

rs144223596 (c.4510C>T) in an isogenic background, which was confirmed by Sanger sequencing

(Fig. S1). Although there was a small C peak visible at rs144223596, this was considered noise,

and as such we considered the clone to be homozygous. Next, the *COL6A3*-edited and the unedited

isogenic control hiPSCs were differentiated into chondrocytes using a previously established

chondrogenic differentiation protocol (*19*). In short, hiPSCs followed a step-wise differentiation

protocol via mesodermal lineage differentiation towards chondroprogenitor cells (*19*). These cells

were then dissociated, and chondrogenesis was initiated in our organoid pellet model.

Characterization of the matrix of isogenic control and COL6A3 mutant hiPSC-derived cartilage

organoids

Successful differentiation towards chondrocytes and the production of neo-cartilage was

confirmed by protein staining of collagen II (COLII), collagen VI (COLVI), and sulfated

glycosaminoglycans (sGAGs) **(Fig. 1A)**. COLII and COLVI deposition was not affected by the

mutation as measured by staining intensity **(Fig. 1B)**. However, quantification of sGAG

deposition, using the dimethyl methylene blue (DMMB) assay normalized to DNA content,

showed a significant reduction in the COLVI-mutant compared to the isogenic control neo-

cartilage organoids (beta=0.55 ± 0.28, P=4.9x10^{-2}) **(Fig. 1C)**. Next, the isogenic and COLVI-

mutant neo-cartilage organoids were characterized by targeted gene expression analysis using RT-

qPCR of markers relevant for cartilage homeostasis and mechano-transduction **(table 1).** The

COL6A3 mutation reduced expression of the catabolic marker *ADAMTS5*, while also reducing

expression of the anabolic markers *COL2A1* as well as *ACAN*.

Transmission electron microscopy of the cartilage neo-matrix

To further investigate the effect of the mutation on the structural properties of the PCM and ECM,

we performed transmission electron microscopy. As shown in **Figure 2A,** there was a reduced

abundance of GAG-like structures in the *COL6A3*-mutant neo-cartilage organoids versus the

isogenic control. Consistent with the DMMB assay, upon performing quantitative analysis of these

GAG-like structures using a deep learning algorithm, we confirmed that mutant COLVI cartilage

had significantly decreased aggregate size (Fig.2B; beta=-479.7, P=1.93X10^{-2}) and GAG

abundance (Fig. 2C; beta=-106.14 ± 14.95, P=2.52X10^{-6}).

Binding of isogenic control and COL6A3 mutant COLVI to pericellular matrix proteins

The identified R1504W mutation is located in the N-terminal domain of COL6A3 coding for a

von Willebrand Factor A domain, which is involved in binding two important proteins in cartilage

PCM and ECM, fibronectin and hyaluronan (*12, 13, 18*). Arginine at this position in the COL6A3

protein is evolutionary highly conserved, indicating that an amino acid change at this position is

likely to affect protein function **(Fig. S2)**. Thus, we hypothesized that the change from a polar

arginine to a non-polar tryptophan affects the interaction between COLVI and PCM/ECM proteins.

Hereto, we have performed a fibronectin and hyaluronan solid-phase binding assay with wild-type

and mutant COLVI, which was extracted from the chondrogenic differentiation medium of neo-

cartilage organoids. Results, as shown in Figure 2, demonstrated that binding to fibronectin was

reduced for mutant COLVI (beta=-0.13 ± 0.06, P=4.37 x10^{-2}). However, we could not detect any

binding of wild-type nor mutant COLVI to hyaluronan in our assay.

Effect of missense COL6A3 mutation on the transcriptomic landscape

Next, using RNA sequencing, we determined the downstream transcriptional effects of these

changes in the PCM and ECM related to the *COL6A3* mutation. The stranded RNA sequencing

allowed us to confirm the genotyping as performed with Sanger sequencing **(Fig S1)**, which

revealed the inclusion of both heterozygous (n=9) and homozygous (n=17) samples in our dataset

To avoid compromising on power in addition to detecting the most robust differentially expressed

genes (DEGs), we have pooled these heterozygous and homozygous samples after correction.

Multifactorial analysis revealed 3700 significant DEGs between the *COL6A3* mutant and isogenic

controls (FDR<0.05) **(Fig. 4A, table S2)**. Among these genes, 55% were upregulated and 45%

were downregulated. Notable highly significant DEGs were related to development and cartilage

metabolism, with the downregulation of structural PCM and ECM proteins, such as *COL27A1*

(FC=0.70, FDR=4x10^{-4}) and *PRG4* (FC=0.21, FDR=1.74x10^{-17}), increased catabolic activity, such

as *MMP9* (FC=3.67, FDR=7x10^{-16}), and ECM mineralization, such as *SPP1* (FC=2.7,

FDR=2.2x10^{-36}) **(Fig. 4A-B)**.

To determine the biological processes associated with the *COL6A3* mutation, we performed a weighted gene co-expression network analysis (WGCNA) (*20*) on the RNA-sequencing data set. This resulted in the detection of 20 distinct co-expression networks **(Fig. S3)**. Multifactorial regression analysis revealed 10 co-expression networks with the first principal component significantly associated with the *COL6A3* genotype **(Fig. S3)**. The top 3 most significant co-expression networks associated with the *COL6A3*-mutant genotype were enriched for developmental processes, cell-cell adhesion/anatomical structure morphogenesis, and ECM organization **(Fig. 4C)**. Enrichment of ECM organization again underlines the detrimental effects of the *COL6A3* mutation on the development of cartilage, affecting genes such as *LAMA5*, *LAMB2*, and *COL18A1* that code for structural PCM components **(Fig. 4D)**. While enrichment of cell-cell adhesion pathways suggests that the mutation also affects mechano-transduction via altered cell-cell adhesion by downregulation of cadherin-associated genes, such as *CDH18*, *CDH6*, *PTGER4*, *MAPK14,* and *ADAMTS5* **(Fig. S4)**. Of note is that *ADAMTS5* is downregulated in the *COL6A3* mutant while quantification of sGAGs, the target peptides of ADAMTS5 cleavage, are reduced at both the gene level (*ACAN*, **Table 1**) and protein level **(Fig. 1C; Fig. 3A-C).**

To study the relevance of the *COL6A3* mutation to OA pathophysiology, we determined the overlap of gene expression between the effects of the *COL6A3* mutation and the differential expression between lesioned and preserved cartilage from patient material collected post-joint replacement surgery in a previously published dataset containing 58 paired samples (*16*) revealing a subset of 582 overlapping DEGs **(table S4)**. We then performed pathway analysis on this subset of genes **(Fig. 4B)**. The most significant enriched pathway was skeletal system development, including transcription factors (*RUNX3*, *TNFRSF11B*), ECM components (such as *COL27A1*, *COL11A2*), and anabolic factors (such as *IGF1*, *BMP3*). Well-known pathways related to

inflammation "inflammatory response" and "acute inflammatory response" were also enriched containing inflammatory cytokines (IL31a) and general inflammatory response factors (*PTGES*, *HLA-e*). Also, the "ossification" pathway was enriched, containing OA risk genes (*SPP1*, *TNC,* and *MGP*). Genes related to cartilage metabolism were confirmed by quantitative reverse transcription polymerase chain reaction (RT-qPCR) **(table S5).** Together, this data suggests that the *COL6A3* mutation results in downstream expression changes, in part describing the osteoarthritis pathophysiology.

Additionally, to explore the effect of the hetero- and homozygous *COL6A3*-mutated hiPSC-derived neo-cartilage organoids, a dose-response effect was modeled for DEGs (FDR<0.05) responding to the *COL6A3* mutation. To this end, the hetero- and homozygous *COL6A3* mutation was considered as a covariate and analyzed for differential expression. This revealed a robust dose-response effect (FDR<0.05) of the *COL6A3* mutation on gene expression in 2610 genes out of the 3700 DEGs affected by the mutation, **(table S6; Figure S6)**, such as MMP9, PRG4, and SPP1 This dose-response effect further underlines the biological validity of the gene expression changes due to *COL6A3* mutation.

Taken together, we showed that the *COL6A3* mutation reduces sGAG deposition **(Fig. 1)**, reduces binding to fibronectin **(Fig. 2)**, and lowers the expression of mechano-sensor genes **(table 1)** suggesting the mutation could affect the transduction of mechanical cues. Hence, we determined whether the *COL6A3* mutation affects the transcriptomic response to hyper-physiologic mechanical loading conditions. Hereto, two different organoid models were applied; cylindrical constructs in which hiPSC-derived pellets were digested to obtain single-cell chondrocytes that were then encapuslated in an agarose gelhydrogel, and spherical constructs with neo-cartilage deposited by hiPSC-derived chondrocytes. Both these organoid models were exposed to hyper-

201 physiologic mechanical loading conditions [20% sinusoidal peak-to-peak strain at 5hz for 10

202 minutes]. Transcriptional activity was measured 12 hours after mechanical stimulation in isogenic

203 controls (unloaded isogenic controls - n=13, mechanically stimulated isogenic controls - n=13) as

204 well as *COL6A3*-mutant (unloaded *COL6A3* mutants – n=14 and mechanically loaded *COL6A3*

205 mutants - n=12) organoids.

Effect of mechanical loading on the transcriptomic landscape

Next, we characterized the effect of hyper-physiologic loading conditions (*21*) on these neo-

cartilage organoids. Multifactorial analyses revealed 177 DEGs (FDR<0.05) between unloaded

and mechanically loaded organoids, of which 74% were upregulated and 26% were downregulated

(Fig.6A, table S7). Notable genes were, amongst others; *CD44* (FC=1.45, FDR=0.019), *CAV1*

(FC=1.52, FDR=4×10^{-4}), *ITGA5* (FC=1.50, FDR=0.021); **Fig. 6B**), which are all genes encoding

for mechano-sensors involved in OA pathophysiology.

To determine the biological processes affected by hyper-physiologic mechanical loading WGCNA

co-expression networks were associated with mechanical loading, revealing 5 significantly

associated co-expression networks **(Fig. S2; table S3)**. The top 3 most significantly associated

modules were enriched for developmental and signaling processes, stress responses**,** and neuronal

pathways **(Fig. 6B)**. While enrichment of signaling responses containing genes such as *IL1RL1*

and *FOSL1* show an adaptive response to hyper-physiologic mechanical loading conditions **(Fig.**

6D), enrichment of stress responses with genes such as *HSPA1B* and *DNAJA4* underlines the

damaging effects of the hyper-physiologic mechanical loading conditions **(Fig 6E).**

Effect of the COL6A3 missense mutation on the response to hyper-physiological mechanical

loading conditions

Finally, the effects of the *COL6A3* mutation on the response to hyper-physiological mechanical

loading were investigated. To this end, a multifactorial analysis was performed resulting in a set

of 135 genes with a significant interaction effect ($P<0.01$) indicating that the mutation affected the

response to hyper-physiological mechanical loading **(table S8)**. Of these 135 genes, 70 proteins

show a significant protein-protein interaction (PPI) (FDR<0.05) as determined by STRING-DB

(Fig. 7A). Notable is that highly connected genes in this PPI network such as; *PTGS2*, *IL1R1*,

IRAK2, *PECAM1*, and *ADAMTS5* are all related to catabolic and inflammatory signaling. *PTGS2*

is known to be regulated by TRPV4 signaling in response to mechanical stress (*22*) and is involved

in inducing an inflammatory response to stimuli (*23*). *IL1R1* codes for the receptor of interleukin-

1, one of the key inflammatory markers in OA, and thus is involved in inflammatory signaling,

while *IRAK2* encodes for the interleukin-1 receptor-associated kinase 2, which is involved in

interleukin-1 (IL-1) induced upregulation of NF-κβ (*24*). Upon performing stratified analysis, it

was shown that the interaction effect was particularly caused by an upregulation of gene expression

observed in isogenic controls in response to hyper-physiological loading conditions, that appeared

absent in the *COL6A3* mutant neo-cartilage organoids **(Figure 7B; table S9).**

To study the biological processes in which the response to hyper-physiological loading differed

between the isogenic control and the *COL6A3* mutants, associate this interaction effect with the

principal component of each detected co-expression network. This revealed three distinct co-

expression networks associated with the interaction effect, which were enriched for processes

related to signaling, ECM organization, and general biological processes **(Figure 7C)**. Enrichment

of pathways related to signaling shows an aberrant response in genes such as *INHBA* which acts

downstream of TRPV4 calcium channels (*22*), *CAV1*, *SEMA7A*, and *MMP3,* which are all genes

that respond to mechanical loading in isogenic controls, with an absent loading effect in the

COL6A3 mutant **(table S3)**. Again, the enrichment of processes related to ECM formation and

organization, containing genes such as; *MMP13, RUNX1, FN1, LAMC1, EGFR,* and *PMEPA1*

(Fig. 7D), underlines the effect of an impaired repair response to hyper-physiological mechanical

loading conditions in the *COL6A3* mutant. Also, the enrichment of general biological processes

including *IL1R1* highlights the aberrant response to mechanical loading in the *COL6A3* mutant

neo-cartilage organoids.

Discussion

Discussion

In the current study, we identified a missense mutation in *COL6A3* (c.4510C>T, p.Arg1504Trp)

in a sibling pair of the GARP-study affected with symptomatic OA in two or more joint sites (*14*).

By introducing this high-impact mutation in hiPSCs using CRISPR-Cas9 genome engineering

while employing these cells in an established 3D *in vitro* neo-cartilage organoid model, we showed

that the mutation decreases cartilage matrix integrity **(Fig. 1C-D**), as reflected by a reduction in

abundance and size of GAGs **(Fig. 2A-C)**. Moreover, by subsequently isolating mutated COL6

protein, we showed that the mutation reduced binding to fibronectin **(Fig. 3)**. Analysis of the

transcriptome-wide gene expression changes with *COL6A3* mutation showed overlap with

transcriptomic changes due to OA-pathophysiology (*16*) **(Fig. 4)** indicating that an osteoarthritic

chondrocyte state appeared secondary to alterations in PCM function due to mutant *COL6A3*.

Finally, by exposing the neo-cartilage organoids to hyper-physiological mechanical stress, we

demonstrated that mutated *COL6A3* abolished the characteristic upregulation of inflammatory

signaling after mechanical loading (*21, 22, 25*) preceding the anabolic response in chondrocytes

(*26, 27*). This was represented by inflammatory markers such as *IL1R1, PECAM1,* and *PTGS2*. In

contrast, other catabolic genes such as *ADAMTS5*, normally being upregulated to hyper-

physiologic mechanical loading conditions (*21*), did not respond to mechanical stress in the

COLVI mutant neo-cartilage organoids. Taken together, these findings suggest that impaired

binding between the PCM proteins COLVI and fibronectin resulted in a particular loss of

proteoglycans, an OA chondrocyte disease state, and abolished the initial stress response to hyper-

physiologic mechanical loading conditions.

Notably, we have explored the effects of the *COL6A3* mutation by challenging the neo-cartilage

organoids with hyper-physiological mechanical loading conditions. Hereto, neo-cartilage

organoids were exposed to 20% deformation at a rate of 5hz, based on previous research showing

a loss of sGAGs, upregulation of catabolic genes, and downregulation of anabolic genes in

response to these mechanical loading conditions (*21*). While we did not observe a statistically

significant loss of sGAGs due to the short-term mechanical loading conditions used in this study

(Fig S6), we observed a marked upregulation of catabolic genes such as; ADAMTS1,3,5 degrading

proteoglycans, MMP3,9 and 13 which degrade COLII fibrils, and MMP25 cleaving fibronectin

(table S9). The fact that we did not observe a loss of sGAGs might be explained by a relatively

lower sensitivity of detecting differential protein expression in comparison to differential gene

expression, but also that protein and gene expression is measured at the same time, possibly

explaining that there is not yet an observed loss of sGAGs or COLII in response to this catabolic

gene-expression profile. However, this catabolic gene-expression profile is overlapping with a

previously published dataset showing upregulation of catabolic genes as well as inflammatory

markers in response to damaging mechanical stress in a human ex-vivo explant model (*28*).

By exposing the cartilage organoids to hyper-physiological mechanical stress to the cartilage organoids, we demonstrated that mutated *COL6A3* abolished the characteristic inflammatory response to hyper-physiological stress (*22*) which precedes regenerative anabolic signaling (*26*). In line with previous experiments, we show that *PTGS2* and *PTGER4*, coding for prostaglandin E2 synthase and the prostaglandin E2 receptor EP4 are upregulated to mechanical stress in the isogenic control organoids while lacking response in the *COL6A3* mutant organoids **(table S9)** (*22, 28, 29*). These PGE2-related genes such as *PTGES* and *PTGS2* were upregulated, similar to OA pathophysiology. However, inhibiting COX2, upstream of PGE2 signaling only has modest effects on pain and disability (*30*), in other tissues, such as epithelium the PGE2 – EP4 axis is essential to initiate a repair in response to stressors (*31*). Also, the interleukin-1 signaling pathway is affected by an ablated upregulation of *IL1R1* and its downstream kinase involved in NF-κβ signaling, *IRAK2*, in response to mechanical loading, possibly explained by being upregulated in the *COL6A3* mutant **(table S10)**. Moreover, matrix-degrading enzymes such as MMP13 and ADAMTS5 which normally are upregulated in response to mechanical loading (*28, 32, 33*) both showed an impaired response to mechanical stress in the *COL6A3* mutant. Of note is that ADAMTS5, the main enzyme cleaving aggrecan, is downregulated in the *COL6A3* mutant, but there is also a decrease in sGAG concentration in the neo-cartilage pellets. One explanation for this opposing observation is that *ADAMTS5* gene expression could be upregulated during matrix deposition in the formation of cartilage in the *COL6A3* mutant, but at the end of the differentiation is down-regulated to attempt to rescue sGAG concentration. While it is tempting to pose that the reduced binding of the mutant COLVI with fibronectin affects the transduction of mechanical cues toward the chondrocytes, more research is needed to confirm this relationship. The fact that the genes showing an interaction effect did not appear differentially expressed upon hyper-

physiological loading in the combined multifactor analysis can be explained by the interaction

effect masking the main effects of hyper-physiological loading. Henceforth, we have applied an

additional stratified analysis of the loading effect in the isogenic controls, showing that indeed

most of these genes respond to mechanical stress **(table S9)**, consistent with previously published

data describing the effects of mechanical loading on gene expression (*21, 22, 28*).

Here, we studied the effect of a high-impact *COL6A3* in hiPSC-derived neo-cartilage organoid

model that had been genome-edited via CRISPR-Cas9 to harbor this mutation. While we initially

concluded, based on sanger sequencing, that our hiPSCs were homozygous, genotyping utilizing

our RNA sequencing data showed that there were also heterozygous samples included. These

heterozygous *COL6A3* mutant cells could have arisen due to a selective advantage upon expanding

hiPSCs. Nonetheless, availability of hetero- and homozygous samples allowed us to study a

possible dose-response effect of the mutation on RNAseq data and confirmed a dose-response

effect in 2610 genes out of the 3700 DEGs. This adds to the validity of our data and biological

relevance of the studied *COL6A3* mutation, as there was an additive effect of the hetero- and

homozygous *COL6A3* mutants on DEGs such as SPP1, MMP9, and PGR4. **(table S6, Fig. S7)**.

We have applied both cylindrical disc-shaped organoids (*22*) as well as spherical pellets (*13, 21*).

The advantage of the first model is an ensured equal distribution of mechanical stress throughout

the disc-shaped sample. The advantage of the second model is that it allows harnessing the original

matrix deposited by the hiPSC-derived chondrocytes thereby permitting the characterization of

changes in the ECM. Combining all samples using multifactor analysis has allowed us to show

that indeed aberrant COLVI function exerts part of its deleterious effects via altered mechano-

transduction of mechanical cues. Additionally, this model of hyper-physiological loading in hiPSC

neo-cartilage organoids can be expanded to define and apply more beneficial mechanical loading

regimes, further unraveling the shift in molecular mechanisms underlying the normal physiological

response to loading that might further aid in the development of treatment strategies.

In contrast to previous findings (*12*), we could not detect any binding of COLVI with hyaluronan,

which might be explained by the source of the COLVI proteins, as they were extracted from the

culture medium. Alternatively, other intermediary proteins are necessary for binding COLVI to

hyaluronan which might not have been present in the medium (*11*). Moreover, we have used TEM

in combination with a, yet to be published, machine-learning tool to detect changes in GAG size

and abundance. The reliability of machine learning tools relies on prudent training of the machine

learning algorithm by correct labeling of the structures to be quantified. Here we relied on the

similarity with previously published data. Nevertheless, the reduced abundance of GAGs as

measured with TEM is in line with the results of the DMMB assay, as well as the Alcian blue

staining **(Fig. 1A-C; Fig. 2A-C)**.

By using genetic engineering of hiPSC-derived neo-cartilage organoids while implementing

hyper-physiological mechanical loading conditions, we are among the first to demonstrate that

aberrant function of COLVI in the PCM, abolishes the initial inflammatory response to hyper-

physiological loading, as marked by, amongst others, changes in *PTGS2* and *PGE4*. Moreover, we

showed that secondary to the COLVI mutation provoked alterations in PCM function,

chondrocytes appeared to enter an OA disease state. The established sustainable methodology

provides an unique framework to determine the role of proteins in the transduction of mechanical

cues from ECM to chondrocytes and to explore ways to modify and/or counteract them. Since

biomechanical cues play a critical role in joint health and disease acquired insights could

eventually contribute to discovery of effective treatment options for OA.

Materials and Methods

Experimental design

The objective of the current study was to study the effects of a likely causal pathogenic mutation, thereby elucidating the effects of aberrant collagen VI functions. Exome sequencing was applied to identify a pathogenic mutation. To study the underlying effect of this mutation, the mutation was introduced in hiPSCs using CRISPR-Cas9 genome engineering, of which a neo-cartilage model was created, followed by mechanical loading and functional analysis.

Exome sequencing

Exome sequencing of a sibling pair with generalized OA at multiple joint sites was performed by Illumina HiSeq 2000 technology (Beijing Genome Institute). The sequences were generated as 100–base pair paired-end reads, after enrichment of 44-Mb exonic sequences by NimbleGen EZ (Roche NimbleGen). Raw imaging files were processed by Illumina base calling software v1.7 with default parameters. SOAPaligner/SOAP2.21 was used to align reads to the GRCh37 reference genome at the UCSC Genome Browser website (http://genome.ucsc.edu/) (*34*).

hiPSC line and cell culture

An hiPSC line as described earlier was used as the unedited isogenic control (*19*). In short, RVR-iPSC line was retrovirally reprogrammed from BJ fibroblasts and characterized. The hiPSCs were maintained under standard conditions (37 °C, 5% CO_2) on Matrigel (Corning) coated plates and

refreshed daily with TeSR-E8 medium (STEMCELL Technologies) upon reaching approximately

70% confluence.

Genome editing of hiPSCs

gRNA targeting *COL6A3* (5'-TCTGAAAACCTACAGATCCC -3') were complexed with Cas9

protein at 25 C for 10-15' and added to a RVR-hiPSC cell suspension of 500K cells in 400 µL

mTeSR to generate the edited hiPSCs. 500 pmol of ssODN (5'-

CTTGCCACAAATTCGAGAGCCTTGCCAGTG

TTCAGTGGGGACCCCCCTCTGAGCCTCAGGCGCCATATGGCGTCCAGCACCGGGGC

GTGGGATCTGTAGGTTTTCAGATAGAATTCTGGGAAGACAT-3') harboring the risk

variant was added to cell suspension. Cells were electroporated with BioRad Gene Pulser system

with the following conditions: [250 V, 750 µF, ∞ Ω, 0.4 cm]. Cells were plated at low density and

colonies were picked to obtain clones derived from single cells. As the risk variant created an

NDEI site, clones were screened by PCR amplification of the risk allele and digestion with NDEI

(New England Biolabs) in CutSmart Buffer for 1 hour at 37C. Successful editing of the targeted

variant was confirmed by Sanger sequencing **(Fig S1)**.

hiPSC differentiation to induced chondrocytes

Generation of induced chondroprogenitor cells (hiCPCs) was based on a protocol previously

described (*19*) which was shown to produce similar neo-cartilage to that produced by human

primary articular chondrocytes (*35*). When hiPSCs reached 60% confluence, the culture medium

was switched to mesodermal differentiation (MD) medium, composed of IMDM GlutaMAX

(IMDM; Thermo Fisher Scientific) and Ham's F12 Nutrient Mix (F12; Sigma-Aldrich) with 1%

chemically defined lipid concentrate (Gibco), 1% insulin/human transferrin/selenous (ITS+;

Corning), 0.5% penicillin-streptomycin (P/S; Gibco), and 450 µM 1-thioglycerol (Sigma-Aldrich).

Before induction of anterior primitive streak (day 0), hiPSCs were washed with wash medium

(IMDM/F12 and 0.5% P/S) and then fed with MD medium supplemented with activin A (30 ng/ml;

Stemgent), 4 µM CHIR99021 (CHIR; Stemgent), and human fibroblast growth factor (20 ng/ml;

FGF-2; R&D Systems) for 24 hours. Subsequently, the cells were washed again with wash

medium, and paraxial mesoderm was induced on day 1, by MD medium supplemented with 2 µM

SB-505124 (Tocris), 3 µM CHIR, FGF-2 (20 ng/ml), and 4 µM dorsomorphin (Tocris) for 24

hours. Before induction of early somite (day 2), cells were washed with wash medium, and then

cells were fed with MD medium supplemented with 2 µM SB-505124, 4 µM dorsomorphin, 1 µM

C59 (Cellagen Technology), and 500 nM PD173074 (Tocris) for 24 hours. Subsequently, cells

were washed with wash medium, and for induction of sclerotome, cells (days 3 to 5) were fed daily

with MD medium supplemented with 2 µM purmorphamine (Stemgent) and 1 µM C59. To induce

chondroprogenitor cells (days 6 to 14), cells were washed briefly with wash medium and fed daily

with MD medium supplemented with human bone morphogenetic protein 4 (BMP-4; 20 ng/ml;

Miltenyi Biotec). Three independent differentiations were done per clone.

Monolayer cultured hiCPC aggregates present at day 14 of the differentiation were washed with

MD medium, dissociated with Gentle Cell dissociation medium (Stem Cell), and centrifuged for

5 min at 1200 rpm. Cell aggregates were subsequently maintained in chondrogenic differentiation

(CD) medium containing Dulbecco's modified Eagle's medium/F12 (Gibco), supplemented with

1% ITS+, 55 µM 2-mercaptoethanol (Gibco), 1% non-essential amino acids (Gibco), 0.5% P/S, L-

ascorbate-2-phosphate (50 µg/ml; Sigma-Aldrich), L-proline (40 µg/ml; Sigma-Aldrich), ML329

(1µM; CSNpharm), C59 (1µM; Tocris), and transforming growth factor–β3 (10 ng/ml; PeproTech)

for 30 days while refreshing medium every 3 to 4 days.

Two different chondrogenic constructs were used for downstream analysis; these chondrogenic

pellets were directly used for further experiments, or they were dissociated using collagenase II,

encapsulated in 2% w/v agarose at 30 million cells/ml, and cultured for 14 days with CD creating

cylindrical shaped constructs.

Mechanical loading

The spherical shaped neo-cartilage constructs were mechanically loaded using a MACH-1

mechanical testing device (Biomomentum), at a rate of 5hz with 20% sinusoidal peak-to-peak

strain for 10 minutes as described earlier (*21*)

sGAG measurement

Sulphated glycosaminoglycan (sGAG) concentrations in the neo-cartilage organoids (µg sGAG/µg

DNA) was measured using the Farndale Dimethyl Methylene Blue (DMMB, Sigma) method (*36*).

Chondroitin sulphate (Sigma) was used as a reference standard. Absorbance was measured at 535

and 595 using a microplate reader (Synergy HT, Biotek). Neo-cartilage sGAG concentrations were

corrected for DNA content measured with the Qubit® 2.0 Fluorometer (Invitrogen™) using the

dsDNA HS Assay Kit (Invitrogen™).

Histology and immunohistochemistry

Neo-cartilage samples were fixed in 4% formaldehyde and embedded in paraffin. Sections were stained with Alcian Blue (Sigma-Aldrich) and Nuclear Fast Red (Sigma-Aldrich). Deposition of collagen II and collagen VI in the neo-cartilage constructs was visualized immunohistochemically. For collagen VI, antigen retrieval was done by treating deparaffinized sections with proteinase K (5 µg/ml, Qiagen) and hyaluronidase (5 mg/ml, Sigma). Sections were incubated overnight with a primary antibody raised against human collagen VI (1:100, abcam), followed by incubation with a HRP conjugated secondary antibody (ImmunoLogic). Peroxidase binding for collagen VI was visualized using diaminobenzidine, and sections were counterstained with haematoxylin.

RT-qPCR

Per sample, two replicate neo-cartilage pellets were collected in TRIzol (Invitrogen™) and RNA was isolated using the RNeasy Mini Kit (Qiagen) according to manufacturer's protocol. DNA contamination was removed by treating the RNA with RNase-Free DNase RNA quality (A260/280: 1.7-2.0) was assessed using the Nanodrop. RNA concentrations were measured with the Qubit® 2.0 Fluorometer (Invitrogen™) using the RNA HS Assay Kit (Invitrogen™)., respectively, with an A260/280 between 1.7-2.0. RNA was reverse transcribed into cDNA using the Transcriptor First Strand cDNA Synthesis Kit (Roche). cDNA was amplified using FastStart SYBR Green Master (Roche) and mRNA expression was measured in triplicates in a MicroAmp™ Optical 384-Well Reaction Plate (ThermoFisher Scientific), using the QuantStudio™ Flex Real-Time PCR system (Applied Biosystems™), with the following cycling conditions: 10 min 95 °C; 10 sec 95 °C, 30 sec 60 °C, 20 sec 72 °C (45 cycles); 1 min 65 °C and 15 sec 95 °C . Primer

efficiency was tested using a cDNA dilution series, and primers were considered efficient with an

efficiency between 90% and 110%. -ΔCt expression levels were calculated using two

housekeeping genes *GAPDH* and *SDHA*, with the following formula: *ΔCt=Ct (gene of interest) –*

Ct (average housekeeping genes). Both housekeeping genes were stably expressed in this model.

Fold changes were calculated using the $2^{-\Delta\Delta Ct}$ method with *ΔΔCt=ΔCt (MS) – ΔCt (Control)*.

RNAseq

RNA from neo-cartilage constructs was extracted 12 hours post mechanical loading. RNA from

spherical neo-cartilage constructs was extracted and processed using a pestle homogenizer in

TRIzol reagent (Invitrogen). RNA was extracted using chloroform, followed by precipitation using

ethanol, and purified with the RNeasy Mini Kit (Qiagen). Genomic DNA was removed by DNase

digestion (Qiagen). Paired-end 2 × 150 base pair RNA sequencing (Illumina NEBNext Ultra II

Directional RNA Library Prep, Illumina NOVAseq 6000) was performed. Strand-specific RNA-

sequencing libraries were generated which yielded on average 25 million reads per sample. Data

from the Illumina platform was analyzed with an in-house pipeline as previously described (*16*).

The adapters were clipped using Cutadapt v1.1. RNA-seq reads were then aligned using GSNAP

against GRCh38 (*37*). Read abundances per sample were estimated using HTSeq count v0.11.1

(*38*) with Ensembl gene annotation version 94. Only uniquely mapping reads were used for

estimating expression. The quality of the raw reads and initial processing for RNA sequencing was

checked using MulitQC v1.9 (*39*). Samples containing > 50% genes with zero values and average

read count < 4 were removed from further analysis. The datasets from both neo-cartilage models

were combined using surrogate variable analysis using the R package SVA version 3.42.0 (*40*).

Outliers where identified (n=2) using hierarchical clustering and principal component analysis

(PCA) which were removed from further analysis. In total, 52 samples were included of which;

isogenic controls (free-swelling isogenic controls=13, mechanically stimulated isogenic

controls=13) as well as COL6A3-mutant (free-swelling COL6A3 mutants=14 and mechanically

loaded COL6A3 mutants, n=12) organoids. Differential expression analysis was performed using

the R package DESeq version 1.34 (*41*). All samples were combined in a multifactorial analysis.

To determine effects of the mutation and hyper-physiological mechanical loading conditions only

the main effects were included into the model. To determine the interaction effect an interaction

term to this model was added. P-values were corrected for their false discovery rate using the

Benjami and Hochman method (*42*). WGCNA analysis was performed using the R package

WGCNA version 1.71 (*20, 43*). A generalized linear model was used to determine the association

between the COL6A3 mutation, hyper-physiological mechanical loading conditions, the

interaction effect and the identified WGCNA co-expression networks. Over representation

enrichment analyses of these co-expression networks using the KEGG, Reactome and gene

ontologie biological processes databases was performed using the anRichment R package version

1.22. Protein-protein network analysis was performed using the online tool STRING version 11.0

(*44*).

Solid-phase binding assay

Conditioned medium of wild-type and *COL6A3* mutant organoids was collected and concentrated

in preparation for the binding assay. To this end, 450 µl of medium was collected in 100 K

molecular weight cutoff Pierce Protein Concentrators (Thermo Scientific) and centrifuged for 10

min at 12,000g. Subsequently, COL6 concentration was determined using the Human COL6A3

ELISA Kit (Assay Genie) according to the manufacturer's protocol.

Clear multiwell plates (R&D Systems) were coated overnight with 100 μl of purified fibronectin

(10 μg/ml; Merck) in phosphate-buffered saline (PBS) at 4°C, followed by four wash steps with

wash buffer (0.05% Tween 20 in PBS). Nonspecific binding was blocked for 1 hour with 3% (w/v)

bovine serum albumin (BSA) in PBS. After washing with wash buffer, the plates were incubated

with 100 μl of concentrated medium samples at COL6A3 concentration of 1.3 ng/ml in assay

buffer (0.05% Tween 20 and 0.5% BSA in PBS) for 2 hours. Plates were then washed four times

with wash buffer and incubated with rabbit anti-COL6A3 biotin-conjugated antibody (Assay

Genie) at 0.2 μg/ml in assay buffer for 1 hour. Plates were washed, after which the plates were

incubated with streptavidin–horseradish peroxidase (Thermo Scientific) at 0.1 μg/ml in assay

buffer for 1 hour. After washing, color development was performed with 100 μl of

tetramethylbenzidine substrate (Thermo Fisher Scientific) for 10 min, reaction was stopped with

100 μl of 1 M HCl, and absorbance was measured at 450 nm. Assays were performed in triplicate.

Transmission electron microscopy

To the neo-cartilage organoids, consisting of cells and matrix, double concentrated fixative was

added to the culture medium resulting in a final concentration of 1,5% glutaraldehyde solution in

0,1M cacodylate buffer. The spheres were kept in fixative for at least an hour at room temperature.

After rinsing 3 times with 0,1M cacodylate buffer the spheres were postfixed in 1% osmium

tetroxide / 1,5% potassium ferricyanide / 0,1M cacodylate buffer at 4°C for an hour. After 3 times

rinsing with 0,1M cacodylate buffer the spheres were divided into 4 quarters. The quarters were

dehydrated in a series of ethanol (70%, 80%, 90% and 100%), followed by an infiltration series

of acetone / EPON LX112 (Ladd Research Industries) mixtures (2:1, 1:1 and 1:2), each step 30

min, and finally in pure EPON LX 112 for 1 hour. The quarters were positioned in a mold with

the wide side towards the cutting surface, filled up with EPON and put in an 70 °C oven to

polymerize for 48 hours.

Ultrathin sections (90 nm) were made with a Leica EM UC6 ultramicrotome and collected on 50

mesh grids. Sections were stained with 7% uranyl acetate in MilliQ for 10 minutes and lead citrate

(*45*). Sections were then imaged in a Tecnai T12 twin (FEI / Thermo Fisher Scientific) with a

Gatan 4kx4k OneView camera (Gatan) at 21.000x magnification (at a pixel size of 1.03 nm) for

machine learning analysis using automated tiled imaging (MyTEM) and images were stitched

together into virtual slides (MyStitch) (*46*).

Image Analysis

For image analysis, in total 18 virtual slides were used from three isogenic control and three

COL6A3 mutant neo-cartilage organoids (3 positions each). Using a custom-written user interface

software (to be published) GAG structures were manually annotated in both control and mutated

samples and from this a model was trained for machine learning. The structures were predicted in

all 18 slides (Fig. S5). Both the surface of the GAGs and their number was extracted from the

predictions.

Statistical analysis

For all data analysis except RNA sequencing we have used a generalized linear model including

the factors hyper-physiological loading and the *COL6A3* mutation using R statistical software

version 4.1.1.

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710   **Competing interests:** F.G. is an employee and shareholder in Cytex Therapeutics Inc. The authors

711   declare that they have no other competing interests.

712   **Data and materials availability:** All data needed to evaluate the conclusions in the paper are

713   present in the paper and/or the Supplementary Materials.

Figures and Tables

Figure 1. Effect of the mutation on neo-cartilage matrix deposition. (A) Representative images

of Alcian blue staining marking sulfated glycosaminoglycans (sGAGs) and immunohistological

staining of collagen II (COL II) and collagen VI (COLVI). Scale bar 200μm. **(B)** Quantification

of Alcian blue, COLII, and COLVI in isogenic control and *COL6A3*-mutant neo-cartilage

organoids showed no significant effect of the mutation (N=16). **(C)** Quantification of sGAG

deposition in neo-cartilage organoids. sGAG deposition in COLVI-mutant neo-cartilage organoids

is reduced in comparison to isogenic controls (beta=0.55 ± 0.28, P=4.9x10^{-2}, N=16). Statistics are

reported as beta ± standard error. The box plots represent 25th, 50th, and 75th percentiles, and

whiskers extend to 1.5 times the interquartile range. Individual samples are depicted by black dots

726 in each graph. P values were attained using a generalized linear model with intensity (for immuno-

727 stainings) and (sGAGs/DNA) as dependent variable and genotype as independent variable.

Figure 2. The COLVI mutation reduces sGAG aggregate size. (A) TEM image of isogenic

control (left) and a *COL6A3*-mutant (right) neo-cartilage organoid. **(B)** Using a deep-learning

algorithm, the sGAG aggregate size was measured, showed a reduction in the *COL6A3*-mutant

neo-cartilage organoids (beta=-479.7, P=1.93×10^{-2}). **(C)** GAG amount was decreased in the

COL6A3-mutant neo-cartilage organoids (beta=-106.14 ± 14.95, P=2.52×10^{-6}). Statistics are

reported as beta ± standard error. The box plots represent 25th, 50th, and 75th percentiles, and

whiskers extend to 1.5 times the interquartile range. Individual samples are depicted by black dots

in each graph. P values were attained using a generalized linear model, with GAG size or

GAGs/mm^2 as a dependent variable and genotype as an independent variable.

Figure 3. The COLVI mutation reduces binding to fibronectin (A) Solid-phase binding assay

with full-length fibronectin-coated wells and wild-type and R1504W mutant COLVI. R1504W

showed a reduced binding to fibronectin (beta=-0.13 ± 0.06, P=4.37 x10^{-2}, N=8). This assay did

not show binding of COLVI to hyaluronan. Statistics are reported as beta ± standard error. The

box plots represent 25th, 50th, and 75th percentiles, and whiskers extend to 1.5 times the

interquartile range. Individual samples are depicted by black dots in each graph. P values were

attained using a generalized linear model with absorbance at 450nm as dependent variable and

genotype as independent variable.

Figure 4. Transcriptomic profile in presence of the *COL6A3* mutation (A) Volcano plot

showing the differentially expressed genes (DEGs) in response to the *COL6A3* mutation (N=26).

Red dots denote DEGs with an FDR<0.05 that are upregulated, and blue dots represent DEGs that

are downregulated, as determined by DESeq2 analysis. **(B)** Notable examples of DEGs between

isogenic control and *COL6A3*-mutant neo-cartilage pellets. The box plots represent 25th, 50th, and

75th percentiles, and whiskers extend to 1.5 times the interquartile range. Individual samples are

depicted by black dots in each graph. ***FDR<0.001 **(C)** Overrepresentation enrichment analysis

(KEGG, REACTOME, GO biological processes) of the top 3 weighted gene co-expression

network analysis (WGCNA) co-expression modules where the first principal component is

significantly associated with the *COL6A3* mutation. **(D)** Pathway – gene network of the enrichment

analysis of the mediumpurple3 cluster. Lines depict the relationship between the genes and the

pathways determined by enrichment analysis. Blue dots depict downregulated DEGs with the

COL6A3 mutation, while red dots depict upregulated DEGs with the *COL6A3* mutation. **(E)**

Overlap between the *COL6A3* mutation DEGs and differential expression between lesioned and

preserved cartilage from a previously published dataset (RAAK study, Ramos et al., 2014). **(F)**

Over-representation enrichment analysis of overlapping DEGs between the mutation and lesioned

versus preserved cartilage. Count depicts the number of genes that are categorized to each pathway.

Figure 5. Chondrogenic models to study the effects of aberrant COLVI function in interaction with hyper-physiologic mechanical loading conditions. hiPSCs in which the

R1504W mutation was introduced using CRISPR-Cas9 genome editing. These cells were

differentiated using an established differentiation protocol to produce neo-cartilage organoids.

Two different organoid models were employed; 1. A spherical pellet model harnessing the original

matrix produced by the hiPSCs. 2. A cylindrical organoid model in which the hiPSc-derived

chondrocytes were embedded in an agarose construct, ideally suited for testing the effects of

mechanical loading conditions. These constructs were both exposed to hyper-physiological

loading conditions, after which the organoids were harvested for downstream analysis.

Figure 6. Transcriptomic profile in response to hyper-physiologic mechanical loading

conditions. (A) Volcano plot of differentially expressed genes (DEGs) in response to hyper-

physiologic loading conditions. Red dots denote differentially DEGs with an FDR<0.05 that are

upregulated, and blue dots represent DEGs that are downregulated as determined by DESeq2

analysis. **(B)** Notable examples of mechano-sensor genes upregulated in response to hyper-

physiological mechanical loading conditions. The box plots represent the 25th, 50th, and 75th

percentiles, and the whiskers extend to 1.5 times the interquartile range. Individual samples are

depicted by black dots in each graph. *FDR<0.05 **(C)** Overrepresentation enrichment analysis

(KEGG, REACTOME, GO biological processes) of the top 3 weighted gene co-expression

network analysis (WGCNA) co-expression modules of which the first principle component is

significantly associated with hyper-physiologic mechanical loading conditions. **(D-E)** Gene-

pathway network of the enrichment analysis of the purple **(D)** and the orangered4 **(E)** co-

expression network where lines depict the relationship between the genes and the pathways

determined by enrichment analysis. Blue dots depict downregulated DEGs in response to hyper-

physiologic mechanical loading conditions, red dots depict upregulated DEGs in response to

hyper-physiologic mechanical loading conditions.

Figure 7. The *COL6A3* mutation affects the biological response to hyper-physiologic loading

conditions. **(A)** Protein-protein interaction (PPI) network based on the STRING-DB of genes that

show an interaction (P<0.01) between the *COL6A3* mutation and hyper-physiological mechanical

loading conditions. Red circles denote an increased response to hyper-physiological mechanical

loading due to the *COL6A3* mutation, while blue circles denote a reduced response to mechanical

stress due to the *COL6A3* mutation (only showing connected nodes). Relative node size depicts

number of connections for each gene within the network **(B)** Examples of central DEGs in the PPI

that are related to an inflammatory response. The box plots represent 25th, 50th, and 75th

percentiles, and whiskers extend to 1.5 times the interquartile range. Individual samples are

depicted by black dots in each graph. **(C)** Gene enrichment analysis of WGCNA hubs significantly

related to the interaction between the *COL6A3* mutation and the response to hyper-physiological

mechanical loading conditions. **(D)** Pathway – gene network of the enrichment analysis of the

purple cluster. Lines depict the relationship between the genes and the pathways determined by

enrichment analysis. Blue and red dots depict, respectively, downregulated and upregulated DEGs

in response to hyper-physiological loading conditions in the isogenic control neo-cartilage

organoids.

Table 1. Effect of the *COL6A3* mutation on markers of cartilage metabolism

Gene	Effect of *COL6A3* genotype		
	beta	SE	*p*-value
Catabolic			
MMP13	0.02	0.27	0.94
MMP3	-1.19	0.70	0.09
ADAMTS5	-1.01	0.14	**<0.001**
Anabolic			
COL2A1	-0.47	0.20	**0.02**
ACAN	-0.54	0.21	**0.01**
Hypertrophic			
COL10A1	-0.07	0.16	0.65