Size tuning of neural response variability in laminar circuits of macaque primary visual cortex

Lauri Nurminen[1,2], Maryam Bijanzadeh[1,3] and Alessandra Angelucci[1,*]

[1] Department of Ophthalmology and Visual Science, Moran Eye Institute, University of Utah, 65 Mario Capecchi Drive, Salt Lake City, UT 84132, USA.

[2] Present address: College of Optometry, University of Houston, 4401 Martin Luther King Boulevard, Houston, TX 77204-2020, USA

[3] Present address: Department of Neurology, UCSF Weill Institute for Neurosciences, University of California San Francisco, San Francisco, CA, USA

[*]Corresponding author's address:

65 Mario Capecchi Drive
Salt Lake City, UT 84132, USA
Tel: (801) 585 7489
Email: alessandra.angelucci@hsc.utah.edu

ABSTRACT

Surround suppression and neural response variability are two widespread cortical phenomena thought to facilitate and impede, respectively, information processing and perception. Typically, manipulations that elicit neural response suppression quench variability, an observation that has led some to suggest that these two phenomena may share a common origin. However, few studies have systematically examined the relationship between surround suppression and variability. Surround suppression is mediated by multiple circuits and mechanisms that depend on the size of the sensory stimulus, and cortical layer. Variability is also laminar dependent. To understand how surround suppression and variability may influence laminar processing, here we have used electrophysiological laminar recordings to examine how neural response variability and the shared variability among neurons are modulated by visual stimulus size across the layers of macaque primary visual cortex (V1). We find that surround suppression does not always quench variability. Instead, variability is tuned for stimulus size in a layer-dependent manner. In all layers, stimulation of the receptive field (RF) reduced neural response variability, and the shared variability among neurons, relative to their pre-stimulus values. As the stimulus was enlarged beyond the RF, to involve the near RF-surround, both neural response variability and shared variability further decreased in infragranular layers, but did not change in granular and supragranular layers. In contrast, larger stimuli involving the far RF-surround increased both neural response variability and shared variability, relative to their value for a stimulus matched to the RF size, in supragranular layers, but decreased them or did not change them in granular and infragranular layers. Surprisingly, we also found that visual stimuli smaller than the RF could increase variability relative to baseline values, particularly in granular and infragranular layers. Our results point to multiple laminar-specific circuits and mechanisms as the source of variability, and call for new models of neural response variability.

INTRODUCTION

Surround suppression and neural response variability are two widespread cortical phenomena thought to affect information processing and perception in seemingly opposite ways. Surround suppression is a non-linear neural response transformation consisting in suppression of a neuron's response to a sensory stimulus presented inside its receptive field (RF) by a stimulus simultaneously presented in the RF surround (Hubel and Wiesel, 1965; Blakemore and Tobin, 1972; Nelson and Frost, 1978; Sceniak et al., 2001; Cavanaugh et al., 2002; Levitt and Lund, 2002; Angelucci and Shushruth, 2013). It is thought to facilitate information processing and the encoding of sensory stimuli, e.g. by facilitating visual perception (Knierim and Van Essen, 1992; Lamme, 1995; Nothdurft et al., 2000), and reducing redundances in sensory inputs (Vinje and Gallant, 2000; Schwartz and Simoncelli, 2001; Haider et al., 2010; Pecka et al., 2014). Neural response variability is the phenomenon in which repeated presentations of an identical visual stimulus produce neuronal spiking responses that differ from trial to trial (Tomko and Crapper, 1974; Vogels et al., 1989), and this trial-to-trial variability is correlated among neurons (Cohen and Kohn, 2011). Traditionally, neural response variability has been interpreted as "noise" that impairs the fidelity of neural representations (Shadlen and Newsome, 1998; Abbott and Dayan, 1999; Averbeck et al., 2006; Moreno-Bote et al., 2014).

It has recently been hypothesized that response suppression (of which surround suppression represents a specific form) and neural variability are intimately connected, and may share a common origin, as manipulations that elicit response suppression typically also quench variability (Goris et al., 2024). However, few studies have systematically examined the relationship between surround suppression and variability. Festa et al. (2021) reported that on average across a population of V1 cells stimuli approximately twice the diameter of the neurons' RF quench variability relative to variability measured for stimuli confined to the RF. However, in this study, individual V1 neurons showed a variety of effects of surround stimulation on variability, including increases, decreases or no effect. A different study showed a decrease in correlated variability among V1 neurons following stimulation of the surround by large stimuli (12° diameter) (Snyder et al., 2014). However, experimental evidence indicates that surround suppression is mediated by multiple circuits and mechanisms, depending on stimulus size, spatio-temporal stimulus configuration and cortical layer (Webb et al., 2005; Angelucci et al., 2017; Bijanzadeh et al., 2018;

Henry et al., 2020). For example, small versus large stimuli presented in the RF surround evoke distinct patterns of laminar activity (Bijanzadeh et al., 2018), consistent with the former engaging intrinsic horizontal connections, which extend into the "near" RF surround of V1 neurons, and the latter corticocortical feedback connections, which are co-extensive with the "far" RF surround of V1 neurons (Angelucci et al., 2002; Angelucci et al., 2017). As previous studies did not systematically address the relationship between stimulus size, single neuron variability and correlated variability, it remains unclear whether near- and far-surround stimulation similarly affect variability, and whether their effects generalize to all cortical layers. Moreover, recent theoretical evidence has demonstrated that not all forms of variability are detrimental to encoding of sensory inputs and perception (Averbeck et al., 2006; Ruff and Cohen, 2014, 2016a; Haefner et al., 2016), and reports that variability is modulated by visual stimuli (Churchland et al., 2010; Ruff and Cohen, 2016a) have led some to suggest that variability may, instead, play a role in sensory information processing. For example, computational studies have assigned a role for variability in perceptual inference (Fiser et al., 2010; Pouget et al., 2013; Orban et al., 2016; Henaff et al., 2020), and suggested that cortical layers may play distinct roles in perceptual inference (Bastos et al., 2012). To obtain a comprehensive understanding of the relationship between surround suppression, variability, and laminar circuits, here we have used electrophysiological laminar recordings to examine how stimulus size affects changes in neural response variability and shared variability across the layers of macaque primary visual cortex (V1). Size tuning experiments allow us to isolate the driving feedforward thalamic inputs to the RF, from the modulatory inputs from the near and far RF surround, carried by intrinsic V1 and corticocortical feedback circuits, respectively (Angelucci et al., 2002, 2017; Nurminen et al., 2018). Understanding this relationship is important to constrain models of cortical circuits and the computations performed by networks of neurons.

We found that surround suppression does not always quench variability. Rather, both single neuron response variability and the shared variability among neurons are tuned for stimulus size, and this size-tuning is layer-dependent. In all layers, a stimulus matched to the RF size of the recorded neurons reduced both variability and shared variability compared to pre-stimulus baseline. However, modulation of variability by stimulation of the RF-surround depended on both stimulus size and cortical layer. In IG layers, a stimulus involving the RF and the near surround decreased both response variability and shared variability, compared to their values for a stimulus

matched to the RF size. Instead, in SG and G layers, near-surround stimulation had small or no effects on variability. A larger stimulus extending farther into the far surround increased variability, relative to its value for stimuli matched to the RF size, in the SG layers, but either did not affect or reduced variability in G and IG layers. Interestingly, we found that in a subset of neurons, particularly in G and IG layers, stimuli smaller than the RF could increase variability compared to pre-stimulus baseline. Our results point to multiple laminar-specific circuits and mechanisms as the source of variability, likely affecting cortical processing and perception in distinct ways, and call for new models of neural response variability.

RESULTS

We recorded visually evoked local field potentials (LFP), single-unit (SU) and multi-unit (MU) spiking activity, using 24-channel linear electrode arrays (100μm electrode spacing) inserted perpendicularly to the surface of area V1 in two sufentanil-anesthetized macaque monkeys (see Methods). For accurate assignment of recorded responses to cortical layers, verticality of the electrode array was verified by the spatial overlap and similarity of orientation preference of the MUs' minimum response fields across the array, and confirmed by postmortem histology (as described in Bijanzadeh et al., 2018). Laminar boundaries were identified by current source density (CSD) analysis of LFP signals (Mitzdorf, 1985) averaged over all stimulus diameters used in this study. This allowed us to locate the granular (G) layer 4C as the site of the earliest current sink followed by a reversal to current source, the site of the reversal marking the bottom of the G layer; layers above and below G were defined as supragranular (SG) and infragranular (IG), respectively. We used spiking activity in response to the same stimulus, to identify the top and bottom of the cortex (Bijanzadeh et al., 2018).

To understand how stimulus size modulates cortical response variability across V1 layers, we measured Fano-factor and the shared variability among simultaneously recorded units as a function of grating diameter for 82 visually responsive MUs, and 60 spike-sorted, visually responsive SUs. At the beginning of each penetration, we mapped the minimum-response fields of the recorded MUs (see Bijanzadeh et al., 2018 for details). We next presented grating stimuli, centered on the aggregate minimum response fields of the recorded MUs, to characterize the

orientation, spatial frequency, and temporal frequency tuning of the recorded MU activity. We then selected the stimulus parameters that maximized the response of the majority of simultaneously recorded MUs across the array. Using these optimized parameters, we ran size tuning experiments in which the diameter of a drifting grating stimulus was varied from 0.1° (0.2° in one penetration) to 26°.

Layer dependent modulation of neural response variability by stimulus size

Figure 1 shows size-tuning data for representative MUs recorded in SG, G, and IG layers. For all three example units, Fano-factor decreased as the stimulus diameter was increased to fill the RF of the recorded neurons. However, for the SG layer MU (**Figure 1A**), increasing the stimulus diameter beyond the RF boundaries increased Fano-factor, relative to Fano-factor measured when the stimulus was matched to the size of the RF. In contrast, increasing the stimulus diameter beyond the RF boundaries did not affect Fano-factor for the G layer MU (**Fig. 1B**). For the IG layer MU, increasing the stimulus diameter beyond the RF led to a further decrease in Fano-factor when the stimulus was approximately twice the size the RF (involving the "near" RF surround), but for larger stimuli (involving the "far" RF surround), Fano factor increased back to approximately its value for a stimulus matched to the RF size (**Fig. 1C**). Similar results were observed for the population of recorded MUs.

Figure 2A shows Fano-factor and mean firing-rate, both normalized to their value evoked by a stimulus diameter equal to the RF diameter (see Methods for definition), averaged over the population of MUs in our sample, separately for the different layers. In SG (n=31 MUs), G (n=15 MUs) and IG (n=36 MUs) layers, increasing the stimulus size up to the RF diameter progressively decreased Fano-factor and increased firing-rate.

Large gratings extending into the RF surround of V1 cells are known to suppress the mean spiking response evoked by a stimulus confined to the cells' RF, a phenomenon known as surround suppression (Sceniak et al., 2001; Angelucci et al., 2002; Cavanaugh et al., 2002; Levitt and Lund, 2002; Shushruth et al., 2009; Angelucci and Shushruth, 2013). Consistent with these previous reports, as the stimulus size was increased beyond that of the RF diameter, firing rate decreased across all layers, and this suppression was strongest in the SG layers. However, increasing the

stimulus diameter beyond the RF of the recorded MUs had different effects on Fano-factor in different layers. In SG and G layers, the minimum Fano-factor was reached for a stimulus the size of the RF diameter; as the stimulus diameter was increased beyond the RF diameter, Fano-factor significantly increased relative to its value for a stimulus matching the RF diameter in SG layers (**Fig. 2A Left)**, but did not significantly change in G layers (**Fig. 2A Middle**). In contrast, in IG layers, the minimum Fano-factor was reached at a stimulus diameter approximately twice the RF diameter (we term this the "near surround"), and beyond this stimulus size, Fano-factor increased back to its value for a stimulus matched to the RF diameter (**Fig. 2A Right**). Size tuning of Fano-factor for individual penetrations is shown in **Figure 2-figure supplement 1.**

To quantify these observations, **Figure 2B** shows Fano-factor estimated at 6 different stimulus diameters individually for each MU (values were extracted from functions fit to the data; see Methods), normalized to its value at a stimulus size matching the RF diameter, and then averaged (geometric mean) over all MUs. Consistent with the population size-tuning curves in **Fig. 2A**, this analysis also showed a laminar dependence of the impact of surround stimulation on Fano-factor.

In SG layers, the normalized Fano-factor was lowest for a stimulus matching the RF diameter, and it begun to increase for stimuli larger than about twice the RF diameter, reaching its maximum (relative to the value at the RF) at the largest stimulus size tested (26°); in SG layers, Fano-factor at 4xRF diameter, 8xRF diameter and 26° diameter was significantly higher than Fano-factor at a stimulus size matching the RF diameter (one sample t-test, $p < 0.05$). Moreover, Fano factor for a stimulus twice the RF diameter was significantly higher from the value measured at RF diameter (one sample t-test, $p = 0.015$).

In IG layers, Fano-factor reached its minimum at a stimulus twice the RF diameter, i.e. extending into the near surround. Fano-factor at 2xRF diameter was significantly lower than Fano-factor for a stimulus matching the RF diameter (one sample t-test, $p = 0.019$) and Fano-factors at 4xRF diameter, 8xRF diameter and 26° diameter were not significantly different from Fano-factor for a stimulus the size of the RF (one sample t-test, $p > 0.45$).

In G layers, Fano-factor reached its minimum for a stimulus the size of the RF diameter and did not change significantly for larger stimuli (one sample t-test $p > 0.19$). Fano-factor for a stimulus twice the RF size was not significantly different from Fano-factor at 26° diameter stimulus ($p = 0.16$, t-test).

Figure 2C plots for each layer the median percent change in Fano-factor, relative to baseline (pre-stimulus), evoked by a stimulus equal in size to the RF diameter of the recorded MUs. In all layers, presentation of visual stimuli in the RF significantly reduced Fano-factor relative to baseline (bootstrap test p<0.03; median±bootstrapped s.e. SG: -34.4±7.55%, n=31; G: -24.3±7.84%, n=14; IG: -13.7±5.99%, n=36). The median percent change in Fano-factor was significantly different in SG layers compared to IG layers (bootstrap test against the null-hypothesis that the medians are equal: p=0.024), but was not significantly different between the other layers (bootstrap test p>0.25).

The impact of near-surround (2xRF diameter) stimulation on Fano-factor was layer dependent. **Figure 2D** plots for each layer the median percent change in Fano-factor evoked by a stimulus matched to the near-surround of each MU, relative to a stimulus matched to the RF diameter. The dots in **Fig. 2D** show this change for individual MUs. Whereas in SG and G layers near surround stimulation did not significantly change Fano-factor, relative to its value for a stimulus matching the RF diameter, in IG layers the percent change in Fano-factor caused by a stimulus in the near surround was significantly different from zero (bootstrap test p=0.010). While near-surround stimulation in all layers could either increase or decrease Fano-factor in individual MUs, in IG layers a greater fraction of the MUs showed percent changes in Fano-factor below zero. We also analyzed the effect on Fano-factor of stimulating the per-neuron surround (**Fig. 2E**, see Methods for definition). Only in the IG layers, the median Fano-factor change evoked by stimulating the per-neuron surround compared to the Fano-factor evoked by RF stimulation differed significantly from zero (bootstrap test, p = 0.01; SG and G layers: bootstrap test, p > 0.17). **Figure 2F** plots for each layer the percent change in Fano-factor evoked by a 26° stimulus (the largest we used) relative to a stimulus matched to the RF diameter. As for the previous analysis, the impact of far surround stimulation on Fano-factor was layer dependent. In G and IG layers, there was no statistically significant change in Fano-factor (median±bootstrapped s.e. G: 7.15±15.6%, bootstrap test median>0: p=0.44; IG: -7.99±3.73%, bootstrap test median<0: p=0.055). In contrast, in SG layers there was a significant increase in Fano-factor as the stimulus involved the "far surround" (SG: 17.4±11.3%, bootstrap test median>0: p=0.04). One MU with extreme change in Fano-factor (564%), caused by dividing with a number close to zero, was removed from the analysis. In summary, near surround stimulation evoked a significant decrease in Fano-factor relative to its value for a stimulus matching the RF in IG layers, but no change in

SG and G layers. Instead, far surround stimulation evoked a significant increase in Fano-factor relative to its value for a stimulus matching the RF in SG layers, but no change in G and IG layers.

Importantly, in all layers individual MUs showed a variety of changes, including increases, decreases or no change in Fano-factor, regardless of whether the near-surround, the per-neuron surround or the entire far surround (26° diameter stimulus) was stimulated; thus, differences in median Fano-factor observed across layers reflected the relative proportion of one vs. another MU type. Thus, for example, the SG layers contained a larger proportion of MUs with far-surround induced increases in Fano-factor than the other layers, but such units were present in all layers. This is demonstrated by the single MU plots shown in **Figs. 2E-F**.

Fig. 2G plots the median normalized stimulus diameter at the lowest Fano-factor value (i.e. at max Fano-factor quenching) in different layers, and the dots indicate this value for each individual MU. Median stimulus diameter at max Fano-factor quenching normalized to the RF diameter was 1.14 (lower and upper bound of the 99% bootstrapped confidence interval of the median: 0.90, 2.42) in SG layers, 1.80 (0.91 19.41) in G layers, and 1.90 (1.32 6.21) in IG layers.

Fig. 2H plots the smallest surround stimulus diameter at max Fano-factor value. For example, for a unit for which surround stimuli of any size reduced Fano-factor or did not change it relative to its value for a stimulus matched to the RF, the stimulus size at max Fano-factor value would correspond to the RF diameter. For SG and G layers, max Fano-factor value occurred when the stimulus diameter was approximately 5 times the RF diameter [median stimulus diameter normalized to the RF diameter and lower and upper bounds of bootstrapped 99% confidence interval, SG: 5.02 (2.93, 32.1); G: 4.84 (1.0, 67.2)]. In contrast, in IG layers max Fano-factor value occurred at a stimulus diameter similar to the RF diameter [1.46 (1.0,4.13)].

To better understand the mechanisms that underlie the effects of surround stimulation on Fano-factor, we investigated whether the surround-induced percent change in Fano-factor linearly depends on the strength of surround suppression. We plotted percent Fano-factor change against suppression index (see Methods) and computed the Pearson's correlation between the two (**Fig. 2I-K**). For near-surround stimulation, the correlation between percent Fano-factor change and suppression index was not significantly different from zero in any of the layers (SG: r=0.25; G: r=0.15; IG: r=0.02; p>0.16; **Fig. 2I**). When the per-neuron surround was stimulated, the correlation was significant in SG layers (r=0.37, p=0.04), but not in G or IG layers (r=0.08 -G-, r=0.22 -IG-, p>0.2; **Fig. 2J**). For far-surround stimulation with a 26° diameter stimulus, the correlation was

significant in SG and IG (r=0.48 -SG-, r=0.50 -IG-, p<0.006), but not G (r=0.30, p=0.30), layers (**Fig. 2K**). In summary, strength of surround suppression was positively correlated with percent change in Fano-factor only for far surround stimulation in SG and IG layers. We also found that surround suppression was stronger in the MUs in which Fano-factor was increased by a 26° diameter grating relative to Fano-factor measured in the RF (one-way ANOVA, strength of surround suppression conditioned on whether RF surround increased, decreased, or had no effect on Fano-factor relative to RF stimulation, p=0.001, n=82). Specifically, for the MUs in which surround stimulation increased Fano-factor relative to RF stimulation (n=21), the strength of surround suppression was 74.1±2.91%, while it averaged 54.7±3.47% for the MUs in which surround stimulation did not affect variability (n=49), and 51.8±5.63% for the MUs in which surround stimulation reduced variability (n=12).

In all layers, statistically significant increases in variability (as determined by bootstrapping; see Methods) induced by surround stimulation had larger magnitude than decreases in variability (increase vs. decrease SG: 103±18.9% vs. -36.5%±6.10%; G: 68.1±14.4% vs. -40.1±20%; IG: 91.6±31.0% vs -36.5±6.09% independent samples t-test pooled over layers and computed over the absolute value of the Fano-factor change induced by RF-surround, p = 0.002).

To rule out that changes in Fano-factor with stimulus size are trivially related to changes in firing rate, we performed a "mean-matched" analysis (Mitchell et al., 2009; Churchland et al., 2010) (see Supplementary Methods, Supplementary Results, and **Figure 2-figure supplement 2**). This analysis showed similar results as described above for the non-mean-matched analysis. One difference between the two analyses was that the mean-matched analysis demonstrated a small but significant decrease in Fano-factor for near-surround stimulation, relative to its value for RF stimulation, also in the G layers (vs. no change in FF for the non-mean-matched analysis; **Fig.2B,D**). Moreover, the mean-matched analysis demonstrated a significant decrease in Fano-factor for far surround stimuli relative to Fano-factor for a stimulus matched to the RF in both the G and IG layers (see Supplementary Results), while there was no difference in Fano-factor between these two stimulus sizes in these layers for the non-mean-matched analysis (**Fig. 2B,F**).

We also replicated this analysis on a smaller population of spike-sorted SUs from SG and IG layers (see Supplementary Methods, Supplementary Results and **Figure 2-figure supplement 3**). Similar to the MU analysis, the SU analysis demonstrated a diversity of responses in all layers (**Fig. 2-figure supplement 3A**). As in MUs, in SUs far surround stimulation in SG layers on

average increased Fano-factor relative to Fano-factor for a stimulus in the RF, but caused no change in IG layers (**Fig. 2-figure supplement 3B,D**). A larger fraction of SUs in both SG and IG layers showed a decrease in Fano-factor for near surround stimuli, relative to Fano-factor for a stimulus matched to the RF diameter (**Fig. 2- figure supplement 3B-C**); this was in contrast to the MU data in which this decrease in Fano-factor for near surround stimulation was only observed in the G and IG layers (**Fig. 2B,D,G**). This was because our larger population of MUs in SG layers contained a larger fraction of individual MUs with lowest Fano-factor value for stimuli matched to the RF size, compared to our smaller population of SUs.

Amplification of cortical response variability by small stimuli

It has been previously reported that the onset of a visual stimulus reduces cortical response variability relative to pre-stimulus baseline (Churchland et al., 2010). However, previous studies used relatively large stimuli, and the impact of stimulus size on response variability has not been explored. Previous experimental studies (Ichida et al., 2007) have shown, and several models of cortical dynamics predicted, that when the cortex is weakly driven (for example by a small stimulus), the cortical state is dominated by excitation, whereas it is dominated by inhibition when the cortex is strongly driven, e.g. by a large stimulus (Schwabe et al., 2006, 2010; Rubin et al., 2015; Hennequin et al., 2018). In an excitation-dominated cortical state, stochastic supralinear stabilized networks predict amplification of response variability relative to pre-stimulus baseline (Hennequin et al., 2018). To test this model's prediction, we examined the impact of small stimuli on response variability.

Figure 3A shows the response of three example MUs to small gratings (0.1-0.6° diameter) centered on the RF. In all three MUs, this small stimulus evoked firing-rates and Fano-factors values higher than those measured during the pre-stimulus baseline.

Amplification of variability for small stimuli was seen also at the population level. **Figure 3B** compares Fano-factor evoked by a 0.1° diameter grating with that evoked by a grating of diameter equal to the RF diameter of the recorded MUs, normalized to the pre-stimulus baseline, and averaged over the population of SG (n=31, left), G (n=15, middle) and IG (n=36, right) MUs. Presentation of the small stimulus significantly increased Fano-factor relative to pre-stimulus baseline in G and IG ($p<0.05$, one-sample t-test, n=15 and 36, respectively), but not SG ($p=0.14$, n=31), layers. Consistent with previous studies (Churchland et al., 2010), in all layers, the larger

stimulus instead decreased Fano-factor relative to baseline. There was no obvious difference in firing-rates across the layers that could have explained the increase in Fano-factor in G and IG layers for smaller stimuli, but not in SG layers.

To provide a better understanding of variability amplification across layers, we performed a MU-by-MU analysis. This revealed significant variability amplification for small stimuli in all layers. We included in this analysis only MUs showing statistically significant increase and decrease (see Methods) in Fano-factor relative to baseline for at least one data-point. While all MUs in our sample showed statistically significant stimulus-evoked decreases in Fano-factor, 67% of these units (55/82) also showed statistically significant increases in Fano-factor for presentation of small stimuli. The proportion of MUs showing both increases and decreases in stimulus-evoked Fano-factors was fairly constant across layers (**SG,** 61%; **G,** 67%; **IG,** 72%).

On average, the largest stimulus-evoked increase in Fano-factor for the cells that showed variability amplification relative to baseline was observed for stimulus diameters smaller than the RF of the recorded MU (**Fig. 3C**; median stimulus diameter normalized to the RF diameter at the largest increase in Fano-factor relative to baseline ± s.d. of the bootstrapped distribution: **SG,** 0.33±1.20; **G,** 0.67±0.52; **IG,** 0.63±0.26). We found that stimulus-evoked increases in Fano-factor were smaller in magnitude than stimulus-evoked decreases in Fano-factor. The difference between the magnitude of maximum variability quenching and magnitude of maximum variability amplification was statistically significant in SG and IG layers (**Fig. 3D**; mean±s.e.m. quenching vs. amplification: **SG,** 1.85±0.37 vs. 0.89±0.14, t-test p=0.01; **IG,** 0.93±0.12 vs. 0.67±0.06, p=0.03), but not in G layers (**G,** 1.14±0.21vs. 0.93±0.19, p=0.23). For this analysis, we removed outlier data points that were at least 2.5 absolute median deviations above or below the median.

Across the entire population, the MUs showing variability amplification for small stimuli (here termed "amplifiers") had a significantly lower baseline Fano-factor than the MUs in which a stimulus always reduced variability (termed "quenchers") (mean baseline Fano-factor±s.e.m.: 3.44±0.33 for quenchers vs. 1.90±0.13 for amplifiers, t-test p=0.000001). However, this varied by layer (**Fig. 3E**); in SG and IG layers, baseline Fano-factor was significantly higher for the quenchers than for the amplifiers (mean baseline Fano-factor±s.e.m.: **SG,** quenchers 4.70±0.39, n=12, vs. amplifiers 2.30±0.29, n=19, t-test p=0.00023; **IG,** quenchers 2.82±0.40, n=10, vs. amplifiers 1.65±0.14, n=26, t-test p=0.0013). Instead, in the **G** layer, baseline Fano-factor did not differ significantly between these two groups (quenchers 1.65±0.14, n=5, vs. amplifiers 1.77±0.19,

n=10, t-test p=0.68). Moreover, baseline firing rate was significantly lower in the amplifiers compared to the quenchers (mean±s.e.m. baseline firing-rate: 4.1±0.4Hz vs. 6.0±0.7Hz, t-test p=2^{-12}). Importantly, however, all amplifiers also showed variability quenching for larger stimuli. This suggests that a floor effect, for example due to low baseline firing-rates, cannot explain the variability amplification in our data (see Discussion). Variability amplification for small stimuli could potentially arise as a result of slow drifting eye movements which can occur under anesthesia. However, we controlled for eye movements by frequent remapping of the minimum response field location (see Methods). **Figure 3-figure supplement 1** rules out eye movements as a potential cause of increased variability for stimuli smaller than the RF size. This figure shows an example penetration in which amplification of variability for small stimuli was seen in 12 MUs, and this amplification could not be explained by eye movements. Because our penetrations were nearly perfectly vertical to the cortical surface (as assessed by alignment of RF location and similarity of tuning functions; see Bijanzadeh et al. 2018 for quantification), eye movements are expected to cause a decrease in firing rate in some trials across the entire cortical depth, i.e. across all contacts in a penetration; this was not observed in the penetration shown in **Figure 3-figure supplement 1.**

Layer dependent size-tuning of network variability

The results presented above indicate that the response variability of visual cortical neurons is modulated by stimulus size. However, the impact of neural response variability on visual processing also depends on how strongly variability is shared across neurons (Shadlen and Newsome, 1998; Bair et al., 2001). To determine the impact of stimulus size on shared variability, we exploited the covariance of simultaneous recordings obtained with electrode arrays.

The left panels in **Figure 4A-C** show raster plots of spiking activity of simultaneously recorded MUs in a single example penetration spanning all layers (SG, n= 4 units, **Fig. 4A**; G, n=3, **Fig. 4B**; IG, n=7, **Fig. 4C**), in response to presentation of gratings of three different diameters (0.1° Top, 0.5° Middle, 26° Bottom). Qualitative inspection of these raster plots reveals that, following presentation of the 0.1° stimulus, the responses of the entire neuronal population waxed and waned in unison. In some trials all MUs spiked vigorously, whereas in other trials the entire population was silent. However, the population responses appeared less coordinated following presentation of the 0.5° diameter grating. The covariation in population responses to presentation

of the 26° diameter grating, instead, appeared to be layer dependent. In all layers, responses to a 26° stimulus were reduced compared to those to a 0.5° diameter grating. However, compared to the responses to the 0.5° stimulus, neural activity in response to the 26° stimulus appeared more strongly coordinated in SG layers, but remained relatively uncoordinated in G and IG layers.

To quantify these observations, we used factor analysis (see Methods). This allowed us to isolate the network variability (i.e. the variability that is shared across MUs) from the private spiking variability (i.e. the variability that is private to each recorded MU) (Churchland et al., 2010). Factor analysis decomposes the measured covariance matrix into a low-rank network covariance matrix and a diagonal matrix that holds the private variances for each MU. Using cross-validated leave-unit-out predictions, we determined that a single-latent dimension was sufficient to model the current data; therefore, we modeled the network covariance matrix with a single factor, and took the diagonal of the network covariance matrix as the shared variance (Churchland et al., 2010). A separate single-factor model was learned for each layer, stimulus condition and penetration. Importantly, the results of this analysis do not imply that V1 activity is one dimensional, but rather reflect the sampled V1 activity. Because we used linear arrays with 100 μm contact spacing, and we factored our analyses based on layer, our sample consists of nearby neurons, at most 700 μm apart. Moreover, to maximize the similarity of the RFs of the recorded neurons, we ensured that the recording probe was inserted vertically into the cortex; this was determined based on the overlap in RF locations, and similarity of the orientation preferences of neurons recorded in a single penetration (for an example penetration, see Fig. 1 in Bijanzadeh et al. 2018).

The right panels in **Figures 4A-C** show the network covariance matrices for the same MUs and three stimulus diameters used for the raster plots. In all layers, shared variance was highest when the smallest of the three stimuli was presented and dropped to near zero in response to the 0.5° stimulus (0.1° vs. 0.5° mean±s.e.m.: SG, 1.53±0.18 vs. 0.48±0.08, n=4; G, 1.07±0.18 vs. 0.16±0.02, n=3; IG, 0.74±0.21 vs. 0.30±0.06, n=7). The impact of larger stimuli on shared variance, instead, depended on layer. Compared to shared variance in response to the 0.5° stimulus, shared variance in response to the 26° stimulus increased in SG layers (0.5° vs. 26° mean±s.e.m.: 0.48±0.08 vs. 0.74±0.20, n=4), did not change in G layers (0.16±0.02 vs. 0.14±0.05, n=3), and decreased in IG layers (0.30±0.06 vs. 0.14±0.04, n=7). The bottom panel of **Figure 4A-C** shows,

for the same example MUs, shared variance as a function of stimulus diameter for all diameters used in our study (0.1-26°).

Figure 5A shows size-tuning of firing rate and shared variance for the population of MUs recorded in SG, G, and IG layers. Shared variance was tuned for stimulus size in a manner that resembled the size tuning of Fano-factor (compare with Fig. 2A). In all layers, increasing the stimulus diameter from 0.1° to a size equal to the aggregate RF diameter of the recorded MUs progressively increased firing-rate, but decreased shared variance (Fig. 5A-B). Shared variance also decreased relative to baseline for a stimulus matched to the RF diameter; the percent change in shared variance was similar across layers and there were no obvious differences across the two animals used in this study (Fig. 5C; median percent change in shared variance±s.d. of the bootstrap distribution, SG: -47.5±11.2%, G: -29.6±18.9%, IG -31.9±17.7). The median percent change in shared variance was significantly below zero in all layers (one-tailed bootstrap test p<0.02). In contrast, the effect on shared variance of stimulating the RF with larger stimuli extending beyond the RF, into the RF surround, differed across layers. Near surround stimulation (2xRF diameter) significantly reduced shared variance compared to its value for a stimulus matched to the RF, only in IG layers, but not in G and SG layers (Fig. 5D; median percent change in shared variance ± s.d. of the bootstrap distribution, SG: -4.60±9.58%, G: -8.31±11.11%, p≥0.21, IG: -28.8±7.01%, p<0.015). Stimulating the per-neuron surround did not affect the shared variance in any layer (Fig. 5E; median percent change in shared variance ± s.d. of the bootstrap distribution, SG: 4.55±20.6%, G: 10.1±20.2%, -37.4±15.5%, p≥0.12). The effect on shared variance of stimulating the far surround with a 26° stimulus differed across layers (Fig. 5F). In SG and G layers, the percent change in shared variance was not significantly different from zero (Fig. 5F; median percent change in shared variance ± s.d. of the bootstrap distribution, SG: 6.35±16.97, G: 7.62±36.43, one-tailed bootstrap test p>0.18). However, in IG layers the 26° diameter stimulus significantly decreased shared variance compared to its value for a stimulus matched to the RF (median percent change in shared variance ± s.d. of the bootstrap distribution -33.7±10.99%, one-tailed bootstrap test p<0.001 (Fig. 5F).

The median stimulus diameter at the lowest shared variance (i.e. at maximum shared variance quenching) normalized to the RF diameter was 1.86 (1.30, 14.7, 99% CI) in SG layers, 2.22 (1.40, 14.9) in G layers, and 6.59 (2.06, 19.9) in IG layers (Fig. 5G).

The median surround stimulus diameter evoking the highest shared variance, normalized to the RF diameter was 5.8 (1.0, 24.4) in SG, 9.4 (2.27, 45.0) in G, and 1.49 (1.0, 6.60) in IG (**Fig. 5H**).

To better understand the connection between shared variance and changes in firing rate related to stimulus size, we computed the average shared variance following the same mean-matching procedure performed for Fano-factor (see Methods). This analysis showed similar results to those of the non-mean matched analysis (see Supplementary Methods and Supplementary Results and **Fig. 5- figure supplement 1**).

DISCUSSION

Using laminar multi-electrode array recordings, we have studied how single neuron response variability and the shared variability among neurons are modulated by stimulus size across the layers of macaque V1. We found that both forms of variability are size-tuned, and this tuning is layer dependent. In all layers, variability declined as a stimulus was progressively increased in size from 0.1° to the diameter of the RF. However, as the stimulus was enlarged beyond the RF, variability changed in a layer and stimulus-size dependent manner. Stimuli involving the near surround decreased variability and shared variability relative to their values for a stimulus the size of the RF, mainly in the IG layers. In contrast, larger stimuli extending into the far surround increased both single neuron and shared variability in SG layers (relative to their value for a stimulus matched to the RF diameter), but did not change them, or reduced them in G and IG layers. Given the hypothesized influence of variability on visual information processing and the encoding of sensory inputs, these laminar differences suggest that the different layers employ different strategies for coding large stimuli. Moreover, given known laminar differences in connectivity, these laminar specific effects of stimulus size on variability suggest different underlying circuit mechanisms.

Theoretical work has shown that correlated variability can be detrimental for sensory processing (Abbott and Dayan, 1999; Averbeck et al., 2006). Consistent with this idea, a number of top-down modulations thought to improve sensory processing and perception tend to reduce spike-count variability (Fano-factor) and correlated variability. For example, attention directed

towards a visual stimulus reduces Fano-factor and correlated variability in primate areas V4 (Cohen and Maunsell, 2009; Mitchell et al., 2009) and V1 (Herrero et al., 2013), decorrelation is induced by perceptual learning in area MSTd (Gu et al., 2011), and surround suppression reduces Fano-factor (Festa et al., 2021) and correlated variability (Snyder et al., 2014) in V1. However, theoretical and experimental work has also indicated that not all correlations impede encoding (Averbeck et al., 2006), that the strength of variability and correlations depends on stimulus, cognitive factors, cortical layers and area (Hansen et al., 2012; Smith et al., 2013; Ruff and Cohen, 2016b, a), and that some form of correlations can facilitate, rather than impede, perception (Ruff and Cohen, 2014; Haefner et al., 2016). In line with these later studies, we find that the effects of surround suppression on variability and correlated variability depend on stimulus size and cortical layer. Our result in IG layers that near and far surround stimulation reduce Fano-factor and correlated variability are consistent with previous reports (Snyder et al., 2014; Orban et al., 2016; Festa et al., 2021) (although we used factor analysis as a measure of shared variability, unlike Snyder et al., which instead measured correlations). However, we have additionally shown that the effect of surround suppression on Fano-factor and shared variability depends on both the size of the surround stimulus (near vs. far) and cortical layer. Unlike in IG layers, in G and SG layers near-surround stimulation did not decrease Fano-factor or shared variability below their values measured for a stimulus matched to the RF size, while far-surround stimulation increased variability in SG layers, but decreased it (or had no effect) in IG layers. As near and far surround suppression are thought to be mediated by different circuits (intra-areal horizontal and inter-areal feedback connections, respectively), and different layers have distinct connectivity, these results suggest that different circuits affect variability in different ways. In particular, they suggest that increased activity of long-range intra-areal or inter-areal feedback connectivity in IG layers quenches variability. In contrast, corticocortical feedback connections to the SG layers may be a source of variability and correlated variability in these layers, and enhancing their activity amplifies variability and correlations. It is unlikely that the increased variability in SG layers induced by presentation of large stimuli is detrimental for visual processing. The impact of surround modulation on visual processing ultimately depends on the way neuronal responses are read out, which may vary with cortical layer. It is also possible that variability increase in SG layers and decrease in IG layers induced by surround stimulation both facilitate encoding and perception. Additional studies are necessary to determine how these laminar-specific modulations of

variability affect perception and behavioral performance, but these laminar differences are consistent with mounting evidence that SG and IG layers represent functionally distinct processing streams. For example, SG and IG layers show distinct dynamics and spectral behavior (Maier et al., 2010; Wang, 2010; Buffalo et al., 2011; Mendoza-Halliday et al., 2024), which are thought to underlie functional and computational asymmetries (Bastos et al., 2012; Shipp, 2016).

It has recently been suggested that variability and response suppression share a common origin, as manipulations that increase response suppression typically quench variability (Goris et al., 2024). Our results, however, indicate that surround suppression is not always associated with variability quenching, as far-surround stimulation in the SG layers increased both variability and shared variability, and instead suggest multiple circuits and mechanisms as the source of variability.

It is often assumed that the trial-to-trial variability of neural responses follows Poisson statistics (Simoncelli et al., 2004). Under Poisson statistics, variability does not depend on firing-rate; rather, Fano-factor remains constant (=1) regardless of mean firing-rate. In contrast, we found that, across all layers, firing-rate increased, and Fano-factor decreased as the stimulus diameter was increased from 0.1° to a diameter equal to that of the RF. These results are inconsistent with the Poisson model of neural response statistics. An extension of the Poisson model, the modulated Poisson model (Goris et al., 2014), augments the Poisson model by a stochastic gain variable. With this addition, the model captures overdispersion (Fano-factor > 1) of neural responses in a physiologically and statistically meaningful way. The modulated Poisson model predicts that Fano-factor increases as firing-rate increases (Goris et al., 2014). In contrast to this prediction, our data shows that for stimuli within the RF, Fano-factor decreases as mean firing-rate increases. Our results for small stimuli resemble those of Solomon and Coen-Cagli (2019) who showed that, in macaque V1, Fano-factor decreased as stimulus contrast (and firing-rate) increased. These authors also concluded that their data was incompatible with the modulated Poisson model and suggested that neural response statistics in macaque V1 are better captured by stochastic normalization models.

A different class of models is based on the idea of perception as probabilistic inference (Knill and Pouget, 2004). In these models, spikes represent samples from probability distributions, and neural response variability reflects the uncertainty of the inferences (Hoyer and Hyvärinen, 2003; Fiser et al., 2010; Orban et al., 2016; Echeveste et al., 2020; Festa et al., 2021). The model

by Festa et al. (2021) predicts a decrease in Fano-factor induced by surround stimulation relative to its value for a stimulus matched in size to the RF. These authors' neural recording results confirmed the model predictions for stimuli extending into the near surround (2xRF size), but for larger stimuli involving the far surround Fano-factor increased back to its value at the RF size. However, these authors did not examine laminar differences, and the use of 1-mm shank length Utah electrode arrays in their study, suggests they may have sampled neurons primarily from the G layer. Our mean-matched analysis confirmed the result of Festa et al. that near-surround stimulation reduces Fano-factor, but we found this to occur only in G and IG layers; we additionally showed that in G and IG layers, as the stimulus was extended into the far surround Fano-factor either increased back to its value at the RF size (non-mean-matched analysis) or remained at its value for a stimulus in the near surround (mean-matched analysis). This points to the intriguing possibility that in G and IG layers, a significant proportion of neurons serves to perform probabilistic inference. Festa et al. (2021) presented also a version of their model in which global context had an additive, instead of multiplicative, effect on neural responses. Interestingly, the additive version of their model predicted that stimulating the RF surround should increase variability, as we found in many cells, particularly in the SG layers.

The laminar differences in variability found in our study suggest different underlying circuit mechanisms and potentially different computational functions. One plausible hypothesis is that laminar-specific inhibitory circuits underlie the different effects of surround stimulation on variability. This hypothesis is based on the assumption that inhibition plays an important role in modulating cortical response variability, as postulated by several models (Stringer et al., 2016; Hennequin et al., 2018; Huang et al., 2019), and the well-established laminar differences in the distribution of inhibitory neuron types (Tremblay et al., 2016). In macaque sensory-motor cortex, somatostatin-positive inhibitory interneurons predominate in SG layers (Hendry et al., 1984; Gielow et al., 2025). In mouse cortex, these interneuron types subtractively control the gain of their target neurons (Sturgill and Isaacson, 2015), by hyperpolarizing the dendrites of pyramidal cells (Markram et al., 2004; Pouille et al., 2013), and mediate surround suppression (Adesnik et al., 2012). This subtractive inhibition counteracts the excitatory feedforward drive (Pouille et al., 2013), thus, ultimately affecting neural responses in a manner resembling reduced feedforward input. Because reduced feedforward input to the cortex increases neural response variability (e.g. Churchland et al., 2010; Festa et al., 2021; and this study), activation of somatostatin neurons

ultimately would lead to increased neural response variability. This hypothesis predicts that neurons in which variability is increased by surround stimulation, which are present in all layers but dominate in the SG layers, are those in which surround suppression is mediated by somatostatin cells. Alternatively, reduced feedforward drive induced by surround stimulation, leading to increased variability, may result from withdrawal of feedforward excitation from surround-suppressed excitatory neurons in the thalamus or cortex itself, a mechanism that is consistent with a recent model of neural response variability (Bressloff, 2019). This hypothesis predicts that neurons in which variability is increased by surround stimulation are those inheriting surround suppression from other suppressed excitatory neurons. In contrast, neurons for which surround stimulation does not affect or decreases variability (more numerous in G and IG layers) may be surround suppressed via different circuit mechanisms; for example, via inhibitory cells that track the activity of excitatory cells (such as parvalbumin interneurons). This mechanism quenches variability in a stochastic inhibition-stabilized network model (Hennequin et al., 2018).

Quenching of cortical response variability by stimulus onset is considered to be a universal property of the cortex (Churchland et al., 2010). In line with this idea, we showed that presenting a stimulus most commonly quenched variability compared to pre-stimulus baseline. However, in addition to variability quenching, we found that, for a substantial fraction of neurons in all layers, but predominantly in G and IG layers, small stimuli amplified variability relative to pre-stimulus baseline. The use of very small stimuli and a unit-by-unit analysis were the key differences between our study and previous studies that did not observe amplification of variability by small stimuli. Amplification of cortical response variability by small visual stimuli relative to pre-stimulus baseline was predicted by a supralinear stabilized network model of cortical response variability (Hennequin et al., 2018). This model predicts variability amplification when the stimulus-evoked response is of comparable magnitude to spontaneous activity. However, in our data, variability amplification was observed also when neural responses were significantly above the spontaneous baseline. Thus, the prediction of supralinear stabilized network models of cortical response variability may not be in quantitative agreement with the results of this study. Variability amplification can trivially arise in units with close to zero baseline firing-rates, as it is often the case for anesthetized primate V1, because the variance of a spike-train with zero mean is necessarily zero and can only increase as the firing-rate increases. In our dataset, the cells that showed variability amplification had lower baseline firing rates and Fano-factor values, but also

showed variability quenching for larger stimuli. Thus, a floor effect due to low baseline firing-rates cannot explain the variability amplification in our data.

A number of different dynamical models have been proposed to explain various aspects of stimulus-dependent variability. In models with multi-stable dynamics, response variability arises from the stochastic wandering across the cortex of spontaneously-formed tuning curves or bumps (Ponce-Alvarez et al., 2013; Bressloff, 2019; Huang et al., 2019). In these models, increased stimulus drive reduces wandering of the activity patterns, locking the stimulus-driven bump in place, and as a consequence quenching variability. Recently, one such model explicitly predicted an increase in variability by surround stimulation (Bressloff, 2019). This prediction is consistent with our results in SG layers, but not in G and IG layers, although this model captures well the experimentally-observed differences in the magnitude of variability across cortical layers in the spontaneous state (Smith et al., 2013). In a different class of models, instead, variability results from fluctuations about a single, stimulus-driven attractor in a stochastic stabilized supralinear network (Hennequin et al., 2018). In these models, when stimulus drive increases, the balanced network causes an increase in inhibition which leads to reduced variability. Thus, in these models, variability quenching results from increased inhibition, as opposed to the multiple-attractor models described above in which variability quenching results from increased excitation. Although the effects of surround suppression on variability have not been explicitly studied in stabilized supralinear network models, they would seem consistent with our results in G and IG layers, i.e. a reduction or saturation of variability by surround stimulation, but not in SG layers.

In summary, existing models of cortical response variability are either inconsistent, or only party consistent with our results, capturing the effects on variability of stimulus size we have observed for some, but not all, layers. We suspect that both kinds of mechanisms may occur, depending on particular cortical operating conditions, and the specific layer. Therefore, our results call for the extension of these existing models or the development of new models that can capture the laminar differences in the stimulus-dependent modulation of cortical response variability we have observed in our study.

MATERIAL AND METHODS

Experimental model

Linear array recordings were made in the parafoveal representation (4-8° eccentricity) of V1 in two anesthetized adult macaque monkeys (*Macaca Fascicularis, 1 male, 1 female*, 3-4 kg). Here we report recordings from a total of 82 visually responsive MUs (82 out of the 120 recorded channels contained a visually responsive MU) from 5 array penetrations. Two of the penetrations were recorded in one animal, and three in the other animal. For the SU analysis, SUs were spike sorted (n=60 SUs; see Supplementary Methods). The data reported in this paper is a subset of the data previously reported in Bijanzadeh et al. (2018). Here, we re-analyzed data from penetrations in which we had collected 21-51 trials per stimulus condition. All experimental procedures were in accordance with protocols approved by the University of Utah Institutional Animal Care and Use Committee and with NIH guidelines.

Surgery

The surgical procedures are described in detail in our previous study (Bijanzadeh et al., 2018). Briefly, anesthesia was induced with ketamine (10 mg/kg, i.m.). An intravenous catheter and endotracheal tube were inserted, the head fixed in a stereotaxic apparatus, and the animal was artificially ventilated with a 70:30 mixture of O_2 and N_2O. End-tidal CO_2, blood O_2 saturation, electrocardiogram, blood pressure, lung pressure, and body temperature were monitored continuously. A small craniotomy and durotomy were performed over the opercular region of V1 and a PVC chamber was glued to the skull surrounding the craniotomy and filled with agar and silicon oil to prevent cortical pulsation and dehydration, respectively. On completion of the surgery, and after a stable plane of anesthesia was reached, the animal was paralyzed with vecuronium bromide (0.3 mg/kg/h, i.v.), to prevent eye movements. Recordings were performed under continuous infusion of sufentanil citrate anesthesia (4-12 µg/kg/h). The pupils were dilated with topical atropine, and the corneas were protected with gas-permeable contact lenses. The eyes were refracted using corrective lenses, and the foveae were plotted on a tangent screen using a reverse ophthalmoscope, and periodically remapped throughout the experiment.

Electrophysiological recordings

To record the activity of V1 SUs and MUs across cortical layers, 24-channel linear arrays (V-Probe, Plexon, Dallas, Texas, 100 µm contact spacing and 20 µm contact diameter) were inserted into area V1, perpendicular to the pial surface to a depth of 2.0-2.2 mm. A custom-made guide tube provided mechanical stability to the array. To facilitate post-mortem visualization of the lesion

tracks, the probes were coated with DiI (Molecular Probes, Eugene, OR) prior to insertion. We recorded extracellularly MU spiking activity and local field potentials (LFP). The signals were amplified, digitized, and sampled at 30 kHz using a 128- system (Cerebus,16-bit A-D, Blackrock Microsystems, Salt Lake City, UT).

Multi-unit selection

MU activity was detected by bandpass filtering continuous voltage traces and thresholding the filtered trace at 4 times the background noise standard deviation, estimated as the median of the continuous recording divided by 0.6745 (Quiroga et al., 2004). The analyses were done only on MUs in which the most strongly driving stimulus evoked at least 3 spikes above the spontaneous activity (count window 50-350 ms after the stimulus onset). Moreover, only MUs in which the response was tuned for stimulus size were analyzed. Whether a unit was statistically significantly tuned for stimulus size was determined by performing ANOVA on the stimulus evoked spike counts. The MUs in which the effect of stimulus size was statistically significant (one-way ANOVA $p < 0.05$) were consider size-tuned.

Visual stimuli

Visual stimuli were generated using Matlab (Mathworks Inc., Natick, MA; RRID:SCR_001622) and presented on a calibrated CRT monitor (Sony, GDM-C520K, 600x800 pixels, 100Hz frame rate, mean luminance $45.7 cd/m^2$, at 57cm viewing distance), and their timing was controlled using the ViSaGe system (Cambridge Research Systems, Cambridge, UK; RRID:SCR_000749). All stimuli were displayed for 500 ms, followed by 750 ms interstimulus interval.

We quantitatively mapped the minimum response field (mRF) of MUs across contacts by flashing a 0.5° black square stimulus over a 3x3° visual field area. The aggregate mRF of the column was defined as the visual field region in which the square stimulus evoked a mean response (+2 s.d. of the stimulus evoked response) that was > 2 s.d. above mean spontaneous activity, and the geometric center of this region was taken as the MUs' aggregate RF center. All subsequent stimuli were centered on this field. We then determined orientation, eye dominance, spatial and temporal frequency preferences of cells across contacts using 1-1.5° diameter drifting sinusoidal grating patches of 100% contrast presented monocularly. Subsequent stimuli were presented at the optimal parameters for most MUs across the column. We measured size tuning across the column

using 100% contrast drifting grating patches of increasing size (0.1-26°) centered over the aggregate mRF of the column. To monitor eye movements, the RFs were remapped by hand approximately every 10-20 minutes and stimuli re-centered on the RF if necessary. To ensure that the array was positioned orthogonal to the cortical surface, we used as criteria the vertical alignment of the mapped mRFs at each contact, and the similarity in the orientation tuning curves across contacts. If RFs were misaligned across contacts, the array was retracted and repositioned.

Quantification and Statistical Analysis

Current Source Density (CSD) analysis

We used CSD responses to small stimuli flashed inside the RFs to identify laminar borders (as detailed in the Results). CSD analysis was applied to the band-pass filtered (1-100Hz) and trial averaged LFP using the kernel CSD toolbox (kCSD_Matlab) (Potworowski et al., 2012). CSD was calculated as the second spatial derivative of the LFP signal. To estimate CSD across layers, we interpolated the CSD every $10\mu m$. The CSD was baseline corrected (Z-scored). In particular, we normalized the CSD of each profile to the s.d. of the baseline (defined as 200ms prior to stimulus onset) after subtraction of the baseline mean (see Bijanzadeh et al. 2018 for details).

Fano-factor

To quantify trial-to-trial variability, we computed Fano-factor by dividing the spike-count variance by the mean spike-count over trials. A small constant (0.0000001) was added to the mean spike-count to avoid dividing by zero. During the course of developing the analysis, we also used a method in which spike-count variance was plotted against mean spike-count computed over trials in 100 ms non-overlapping bins, and by fitting to the variance-to-mean curves a line so that the intersection of the line and the y-axis was constrained to be zero and the slope of the line was taken as the Fano-factor. All findings of the study were replicated using both methods, but we chose the direct division for convenience as it allows for more efficient bootstrapping of errors. All of our analyses were performed between 50 to 450 ms after stimulus onset, except for the pre-stimulus baseline that was computed from -400 to 0 ms before stimulus onset.

To determine the significance of the different effects of surround stimulation on Fano-factor (the data in **Fig. 2D-F**), we re-sampled % change in Fano-factors 9999 times with replacement

from a distribution with zero median, and computed the proportion of samples in which the % change was larger than the observed values.

To determine whether a stimulus caused a statistically significant increase or decrease in Fano-factor relative to baseline in MUs (the analyses presented in **Fig. 3**), the distribution of the difference between Fano-factor and baseline at each stimulus size was resampled with replacement 3000 times. The mean of this distribution was set to zero. If the Fano-factor measured at a given stimulus diameter was higher (smaller) than the 95th (5th) percentile of this distribution, we concluded that the stimulus significantly increased (decreased) Fano-factor relative to baseline.

For details on the mean-matched Fano-factor analysis see Supplementary Methods.

Function fitting, receptive field and surround size and suppression index

To estimate the size of the RF center and surround for each unit, we measured size tuning as described above and plotted the mean firing rate of the unit against stimulus diameter; we, then, fitted these data with ratio-of-Gaussians functions (Cavanaugh et al., 2002). The Fano-factor data was fitted with two ratio-of-Gaussians functions that were summed. These two ratio-of-Gaussians functions had independent parameters. The parameters were optimized by minimizing the squared difference between the function and the data. For firing-rate, the minimization was performed with the Levenberg-Marquardt algorithm as implemented in SciPy (Virtanen et al., 2020). The parameters of the function were constrained to be positive, including zero. For Fano-factor, the parameters of the function were fitted with the basinhopping algorithm as implemented in Scipy. As the sum of two ratio-of-Gaussians function was overfitting the data, we constrained the parameters to be always positive with an upper bound between 1 and 100, depending on the parameter. With these constraints, the fitted functions were always smooth. Two ratio-of-Gaussians functions were also fitted to the shared variance data.

From the fitted functions, the size of the RF center was taken to be the stimulus diameter at which the function peaked. The "per-neuron" surround size was taken to be the smallest stimulus diameter, larger than the RF size, at which the slope of the fitted size-tuning function was at least 10% higher than the minimum slope of the curve. The slope was computed at all stimulus sizes between the RF size and 26°. We used this "unconventional" measure of surround size because, compared to conventional measures, it seemed to better match qualitative estimates of surround

size obtained by manual inspection of the data. Surround sizes obtained with this methods were, however, very similar to those obtained by conventional measures.

The suppression index, used to quantify the strength of surround suppression in **Fig. 2I-K** was defined as $SI=(R_{RF} - R_{SUR}) / R_{RF}$, where R_{RF} is the response at the RF size and R_{SUR} is the response at a grating diameter of 26°, extracted from the fitted functions. The SI equals zero when there is no surround suppression and 1 when the response is completely suppressed.

Factor Analysis

We used factor analysis to decompose the trial-to-trial spike-count covariance matrix into private (single neuron spiking variability) and shared (network) components. Factor-analysis was separately performed for each penetration, stimulus condition, and layer. A 300 ms-window was used. The covariance matrices were modeled as the product of the factor loading matrix and its transpose, plus a diagonal matrix containing the variances that are private to each unit. The matrix of factor loadings and the diagonal private variance matrix were estimated with the Gaussian-process factor analysis toolbox of Yu et al. (2009). As an estimate of the shared variance for each unit, we used the diagonal components of the matrix that results from multiplying the factor loading matrix with its own transpose.

To choose the latent space dimensionality of the model, we performed 5-fold cross validation separately for each stimulus condition. For each cross-validation fold, we performed a leave-neuron-out prediction for all neurons and computed the root-mean-square error (RMSE) of the prediction with respect to the recorded spike counts (Yu et al., 2009). The RMSE was then averaged over cross validation folds. In SG layers, at most stimulus diameters, the RMSE decreased as the latent space dimensionality increased from 1 to 2. However, the decrease was not statistically significant (t-test, $p > 0.05$). In G layers, the RMSE vs. latent space dimensionality curves were essentially flat. In IG layers at all stimulus diameters, RMSE monotonically increased as the latent space dimensionality was increased. Thus, as there was not sufficient evidence in favor of more than one dimensional latent space, we chose to model our data with one latent space dimension.

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COMPETING INTERESTS

The authors declare no competing interests.

REFERENCES

1.   Abbott LF, Dayan P (1999) The effect of correlated variability on the accuracy of a population code. Neural Comput 11:91-101.

2.   Adesnik H, Bruns W, Taniguchi H, Huang ZJ, Scanziani M (2012) A neural circuit for spatial summation in visual cortex. Nature 490:226-231.

3.   Angelucci A, Shushruth S (2013) Beyond the classical receptive field: surround modulation in primary visual cortex. In: The new visual neurosciences (Chalupa LM, Werner JS, eds), pp 425-444. Cambridge: MIT press.

4.   Angelucci A, Levitt JB, Walton E, Hupé JM, Bullier J, Lund JS (2002) Circuits for local and global signal integration in primary visual cortex. J Neurosci 22:8633-8646.

5.   Angelucci A, Bijanzadeh M, Nurminen L, Federer F, Merlin S, Bressloff PC (2017) Circuits and mechanisms for surround modulation in visual cortex. Ann Rev Neurosci 40:425-451.

6.   Averbeck BB, Latham PE, Pouget A (2006) Neural correlations, population coding and computation. Nat Rev Neurosci 7:358-366.

7.   Bair W, Zohary E, Newsome WT (2001) Correlated firing in macaque visual area MT: time scales and relationship to behavior. J Neurosci 21:1676-1697.

8.   Bastos AM, Usrey WM, Adams RA, Mangun GR, Fries P, Friston KJ (2012) Canonical microcircuits for predictive coding. Neuron 76:695-711.

9.   Bijanzadeh M, Nurminen L, Merlin S, Angelucci A (2018) Distinct laminar processing of local and global context in primate primary visual cortex. Neuron 100:1-16.

10.   Blakemore C, Tobin EA (1972) Lateral inhibition between orientation detectors in the cat's visual cortex. Exp Brain Res 15:439-440.

11.   Bressloff PC (2019) Stochastic neural field model of stimulus-dependent variability in cortical neurons. PLoS Comput Biol 15:e1006755.

12.   Buffalo EA, Fries P, Landman R, Buschman TJ, Desimone R (2011) Laminar differences in gamma and alpha coherence in the ventral stream. Proc Natl Acad Sci USA 108:11262-11267.

13.   Cavanaugh JR, Bair W, Movshon JA (2002) Nature and interaction of signals from the receptive field center and surround in macaque V1 neurons. J Neurophysiol 88:2530-2546.

14.   Churchland MM et al. (2010) Stimulus onset quenches neural variability: a widespread cortical phenomenon. Nat Neurosci 13:369-378.

15. Coen-Cagli R, Solomon SS (2019) Relating Divisive Normalization to Neuronal Response Variability. J Neurosci 39:7344-7356.

16. Cohen MR, Maunsell JH (2009) Attention improves performance primarily by reducing interneuronal correlations. Nat Neurosci 12:1594-1600.

17. Cohen MR, Kohn A (2011) Measuring and interpreting neuronal correlations. Nat Neurosci 14:811-819.

18. Echeveste R, Aitchison L, Hennequin G, Lengyel M (2020) Cortical-like dynamics in recurrent circuits optimized for sampling-based probabilistic inference. Nat Neurosci 23:1138-1149.

19. Festa D, Aschner A, Davila A, Kohn A, Coen-Cagli R (2021) Neuronal variability reflects probabilistic inference tuned to natural image statistics. Nature Communications 12:1-11.

20. Fiser J, Berkes P, Orban G, Lengyel M (2010) Statistically optimal perception and learning: from behavior to neural representations. Trends Cogn Sci 14:119-130.

21. Gielow M, Federer F, Jayakumar A, Caldwell Z, Winebrenner C, Xu X, Angelucci A (2025) Laminar specificity and coverage of enhancer-AAV-mediated gene expression restricted to subpopulations of Somatostatin and Parvalbumin inhibitory interneurons in primate V1. Soc Neurosci Abstr Online.

22. Goris RL, Movshon JA, Simoncelli EP (2014) Partitioning neuronal variability. Nat Neurosci 17:858-865.

23. Goris RLT, Coen-Cagli R, Miller KD, Priebe NJ, Lengyel M (2024) Response sub-additivity and variability quenching in visual cortex. Nat Rev Neurosci 25:237-252.

24. Gu Y, Liu S, Fetsch CR, Yang Y, Fok S, Sunkara A, DeAngelis GC, Angelaki DE (2011) Perceptual learning reduces interneuronal correlations in macaque visual cortex. Neuron 71:750-761.

25. Guillory KS, Normann RA (1999) A 100-channel system for real time detection and storage of extracellular spike waveforms. J Neurosci Methods 91:21-29.

26. Haefner RM, Berkes P, Fiser J (2016) Perceptual Decision-Making as Probabilistic Inference by Neural Sampling. Neuron 90:649-660.

27. Haider B, Krause MR, Duque A, Yu Y, Touryan J, Mazer JA, McCormick DA (2010) Synaptic and network mechanisms of sparse and reliable visual cortical activity during nonclassical receptive field stimulation. Neuron 65:107-121.

28. Hansen BJ, Chelaru MI, Dragoi V (2012) Correlated variability in laminar cortical circuits. Neuron 76:590-602.

29.   Henaff OJ, Boundy-Singer ZM, Meding K, Ziemba CM, Goris RLT (2020) Representation of visual uncertainty through neural gain variability. Nat Commun 11:2513.

30.   Hendry SH, Jones EG, Emson PC (1984) Morphology, distribution, and synaptic relations of somatostatin- and neuropeptide Y-immunoreactive neurons in rat and monkey neocortex. J Neurosci 4:2497-2517.

31.   Hennequin G, Ahmadian Y, Rubin DB, Lengyel M, Miller KD (2018) The Dynamical Regime of Sensory Cortex: Stable Dynamics around a Single Stimulus-Tuned Attractor Account for Patterns of Noise Variability. Neuron 98:846-860 e845.

32.   Henry CA, Jazayeri M, Shapley RM, Hawken MJ (2020) Distinct spatiotemporal mechanisms underlie extra-classical receptive field modulation in macaque V1 microcircuits. Elife 9:e54264.

33.   Herrero JL, Gieselmann MA, Sanayei M, Thiele A (2013) Attention-induced variance and noise correlation reduction in macaque V1 is mediated by NMDA receptors. Neuron 78:729-739.

34.   Hoyer P, Hyvärinen A (2003) Interpreting neural response variability as Monte Carlo sampling of the posterior. In: Advances in Neural Information Processing Systems (Becker S, ed), pp 277-284: MIT Press.

35.   Huang C, Ruff DA, Pyle R, Rosenbaum R, Cohen MR, Doiron B (2019) Circuit Models of Low-Dimensional Shared Variability in Cortical Networks. Neuron 101:337-348 e334.

36.   Hubel DH, Wiesel TN (1965) Receptive fields and functional architecture in two nonstriate visual areas (18 and 19) of the cat. J Neurophysiol 28:229-289.

37.   Ichida JM, Schwabe L, Bressloff PC, Angelucci A (2007) Response facilitation from the "suppressive" receptive field surround of macaque V1 neurons. J Neurophysiol 98:2168-2181.

38.   Knierim JJ, Van Essen D (1992) Neuronal responses to static texture patterns in area V1 of the alert macaque monkey. J Neurophysiol 67:961-980.

39.   Knill DC, Pouget A (2004) The Bayesian brain: the role of uncertainty in neural coding and computation. Trends Neurosci 27:712-719.

40.   Lamme VAF (1995) The neurophysiology of figure-ground segregation in primary visual cortex. J Neurosci 15:1605-1615.

41.   Levitt JB, Lund JS (2002) The spatial extent over which neurons in macaque striate cortex pool visual signals. Vis Neurosci 19:439-452.

42.   Maier A, Adams GK, Aura C, Leopold DA (2010) Distinct superficial and deep laminar domains of activity in the visual cortex during rest and stimulation. Front Syst Neurosci 4:31.

43. Markram H, Toledo-Rodriguez M, Wang Y, Gupta A, Silberberg G, Wu C (2004) Interneurons of the neocortical inhibitory system. Nat Rev Neurosci 5:793-807.

44. Mendoza-Halliday D, Major AJ, Lee N, Lichtenfeld MJ, Carlson B, Mitchell B, Meng PD, Xiong YS, Westerberg JA, Jia X, Johnston KD, Selvanayagam J, Everling S, Maier A, Desimone R, Miller EK, Bastos AM (2024) A ubiquitous spectrolaminar motif of local field potential power across the primate cortex. Nat Neurosci 27:547-560.

45. Mitchell JF, Sundberg KA, Reynolds JH (2009) Spatial attention decorrelates intrinsic activity fluctuations in macaque area V4. Neuron 63:879-888.

46. Mitzdorf U (1985) Current source-density method and application in cat cerebral cortex: investigation of evoked potentials and EEG phenomena. Physiol Rev 65:37-100.

47. Moreno-Bote R, Beck J, Kanitscheider I, Pitkow X, Latham P, Pouget A (2014) Information-limiting correlations. NatNeurosci 17:1410-1417.

48. Nelson JI, Frost B (1978) Orientation selective inhibition from beyond the classical visual receptive field. Brain Res 139:359-365.

49. Nothdurft HC, Gallant JL, Van Essen DC (2000) Response profiles to texture border patterns in area V1. Vis Neurosci 17:421-436.

50. Nurminen L, Merlin S, Bijanzadeh M, Federer F, Angelucci A (2018) Top-down feedback controls spatial summation and response amplitude in primate visual cortex. Nature Commun 9:2281.

51. Orban G, Berkes P, Fiser J, Lengyel M (2016) Neural Variability and Sampling-Based Probabilistic Representations in the Visual Cortex. Neuron 92:530-543.

52. Pachitariu M, Steinmetz N, Kadir S, Carandini M, Harris KD (2016) Kilosort: realtime spike sorting for extracellular electrophysiology with hundreds of channels. BioRxiv:https://doi.org/10.1101.061481.

53. Pecka M, Han Y, Sader E, Mrsic-Flogel TD (2014) Experience-dependent specialization of receptive field surround for selective coding of natural scenes. Neuron 84:457-469.

54. Ponce-Alvarez A, Thiele A, Albright TD, Stoner GR, Deco G (2013) Stimulus-dependent variability and noise correlations in cortical MT neurons. Proc Natl Acad Sci U S A 110:13162-13167.

55. Potworowski J, Jakuczun W, Leski S, Wojcik D (2012) Kernel current source density method. Neural Comput 24:541-575.

56. Pouget A, Beck JM, Ma WJ, Latham PE (2013) Probabilistic brains: knowns and unknowns. Nat Neurosci 16:1170-1178.

57. Pouille F, Watkinson O, Scanziani M, Trevelyan AJ (2013) The contribution of synaptic location to inhibitory gain control in pyramidal cells. Physiol Rep 1:e00067.

58. Quiroga RQ, Nadasdy Z, Ben-Shaul Y (2004) Unsupervised spike detection and sorting with wavelets and superparamagnetic clustering. Neural Comput 16:1661-1687.

59. Rosenbaum R, Smith MA, Kohn A, Rubin JE, Doiron B (2017) The spatial structure of correlated neuronal variability. Nat Neurosci 20:107-114.

60. Rubin DB, Van Hooser SD, Miller KD (2015) The stabilized supralinear network: a unifying circuit motif underlying multi-input integration in sensory cortex. Neuron 85:402-417.

61. Ruff DA, Cohen MR (2014) Attention can either increase or decrease spike count correlations in visual cortex. Nat Neurosci 17:1591-1597.

62. Ruff DA, Cohen MR (2016a) Stimulus Dependence of Correlated Variability across Cortical Areas. J Neurosci 36:7546-7556.

63. Ruff DA, Cohen MR (2016b) Attention Increases Spike Count Correlations between Visual Cortical Areas. J Neurosci 36:7523-7534.

64. Sceniak MP, Hawken MJ, Shapley RM (2001) Visual spatial characterization of macaque V1 neurons. J Neurophysiol 85:1873-1887.

65. Schwabe L, Obermayer K, Angelucci A, Bressloff PC (2006) The role of feedback in shaping the extra-classical receptive field of cortical neurons: a recurrent network model. J Neurosci 26:9117-9129.

66. Schwabe L, Ichida JM, Shushruth S, Mangapathy P, Angelucci A (2010) Contrast-dependence of surround suppression in Macaque V1: experimental testing of a recurrent network model. Neuroimage 52:777-792.

67. Schwartz O, Simoncelli EP (2001) Natural signal statistics and sensory gain control. Nat Neuroscience 4:819-825.

68. Shadlen MN, Newsome WT (1998) The variable discharge of cortical neurons: implications for connectivity, computation, and information coding. J Neurosci 18:3870-3896.

69. Shipp S (2016) Neural Elements for Predictive Coding. Front Psychol 7:1792.

70. Shushruth S, Ichida JM, Levitt JB, Angelucci A (2009) Comparison of spatial summation properties of neurons in macaque V1 and V2. J Neurophysiol 102:2069-2083.

71. Simoncelli EP, Paninski L, Pillow J, Schwartz O (2004) Characterization of neural responses with stochastic stimuli. In: The New Cognitive Neurosciences (Gazzaniga M, ed): MIT Press.

72. Smith MA, Jia X, Zandvakili A, Kohn A (2013) Laminar dependence of neuronal correlations in visual cortex. Journal of neurophysiology 109:940-947.

73. Snyder AC, Morais MJ, Kohn A, Smith MA (2014) Correlations in V1 are reduced by stimulation outside the receptive field. J Neurosci 34:11222-11227.

74. Stringer C, Pachitariu M, Steinmetz NA, Okun M, Bartho P, Harris KD, Sahani M, Lesica NA (2016) Inhibitory control of correlated intrinsic variability in cortical networks. Elife 5:e19695.

75. Sturgill JF, Isaacson JS (2015) Somatostatin cells regulate sensory response fidelity via subtractive inhibition in olfactory cortex. Nat Neurosci 18:531-535.

76. Tomko GJ, Crapper DR (1974) Neuronal variability: non-stationary responses to identical visual stimuli. Brain Res 79:405-418.

77. Tremblay R, Lee S, Rudy B (2016) GABAergic Interneurons in the Neocortex: From Cellular Properties to Circuits. Neuron 91:260-292.

78. Vinje WE, Gallant JL (2000) Sparse coding and decorrelation in primary visual cortex during natural vision. Science 287:1273-1276.

79. Virtanen P et al. (2020) SciPy 1.0: fundamental algorithms for scientific computing in Python. Nat Methods 17:261-272.

80. Vogels R, Spileers W, Orban GA (1989) The response variability of striate cortical neurons in the behaving monkey. Exp Brain Res 77:432-436.

81. Wang XJ (2010) Neurophysiological and computational principles of cortical rhythms in cognition. Physiol Rev 90:1195-1268.

82. Webb BS, Dhruv NT, Solomon SG, Tailby C, Lennie P (2005) Early and late mechanisms of surround suppression in striate cortex of macaque. J Neurosci 25:11666-11675.

83. Yu BM, Cunningham JP, Santhanam G, Ryu SI, Shenoy KV, Sahani M (2009) Gaussian-process factor analysis for low-dimensional single-trial analysis of neural population activity. J Neurophysiol 102:614-635.

FIGURE LEGENDS

Figure 1. Size tuning of Fano-factor and mean firing rate in macaque V1: representative units. (A) Representative supragranular (SG) layer unit. **Left:** MU spike-rasters measured at two stimulus diameters, either a diameter equal to the RF diameter of the recorded MU (Top), or a diameter of 26° (Bottom). **Middle**: Peri-stimulus time histograms (PSTHs) of Fano-factor (*red*) and mean firing-rate (*black*) computed in a 100 ms rectangular sliding window for the same two stimulus diameters. The *shaded area* represents the standard deviation (s.d.) of the bootstrapped Fano-factor distribution (for the Fano-factor curve) or the standard-error-of-the-mean (s.e.m., for the firing rate curve). *Inset***:** Zoomed-in Fano-factor curves for the smaller (*darker red*) and larger (*lighter red*) stimulus diameters between 50 and 350 ms after stimulus onset. **Right**: Fano-factor (*red*) and firing-rate (*black*) averaged over 50-350 ms after stimulus onset and plotted against the stimulus diameter. *Solid lines*: fits to the data. *Dashed lines*: baseline Fano-factor (*red)* and firing rate (*black*), measured prior to stimulus onset. Error bars are: s.d. of the bootstrapped Fano-factor distribution (*red*) or s.e.m. (*black*). **(B)** Representative granular (G) layer unit. **(C)** Representative infragranular (IG) layer unit. Conventions in (B-C) are as in (A).

Figure 2. Size tuning of Fano-factor and mean firing rate: MU population data. (A) Average Fano-factor (*red*) and mean firing-rate (*black*) as a function of stimulus diameter for the population of SG (**Left**; n=31), G (**Middle**; n=15) and IG (**Right**; n=36) layer MUs. *Dashed lines*: average baseline Fano-factor (*red)* and firing rate (*black*); error bars: s.d. of the bootstrap distribution. Before averaging, stimulus diameter, Fano-factor and firing-rate of each multi-unit were normalized to the value at the RF diameter. **(B) Top:** RF-normalized Fano-factor values averaged separately for six stimulus diameters: 0.1° or 0.2° (depending on which was the smallest diameter used for that penetration), a diameter equal to the RF diameter, a diameter twice the RF diameter (near surround), four times the RF diameter, eight times the RF diameter and 26°. Error bars: s.d. of the bootstrap distribution. **Bottom:** Box plots of normalized Fano-factor for MUs in SG, G, and IG layers at the same six stimulus diameters as shown in the top panel. *Dots*: Fano-factor values for individual MUs; *red horizontal lines*: medians. The extent of the box marks the inter-quartile range of the data, and the whiskers mark the extent of the entire distribution, save for outliers that were outside 1.5 times the inter-quartile range. **(C)** Median percent change in Fano-factor relative

to baseline induced by a stimulus matched in size to the RF diameter, for the different layers. *Dots:* Individual data points. Error bars (red): s.d. of the bootstrap distribution. *Black and white dots* indicate data from different animals (case numbers indicated in panel D). **(D)** Median percent change in Fano-factor induced by a stimulus twice the RF diameter (near surround) relative to the Fano-factor value evoked by a stimulus matched to the RF diameter. Other conventions as in panel C). **(E)** Median percent change in Fano-factor induced by a stimulus with diameter equal to the surround diameter for individual cells (see Methods), relative to the Fano-factor value evoked by a stimulus matched to the RF diameter. Other conventions as in panel (C). **(F)** Median percent change in Fano-factor induced by a 26° diameter stimulus, relative to the Fano-factor value evoked by a stimulus matched to the RF diameter. Other conventions as in panel (C). **(G)** Median stimulus diameter at the smallest Fano-factor value (or max quenching), normalized to the RF diameter of each recorded MU, for different layers. Error bars: s.d. of the bootstrapped distributions. *Dots:* individual MUs. **(H)** Median surround stimulus diameter at the highest Fano-factor value, normalized to the RF diameter. A value of 1 indicates that the highest Fano-factor value occurred at a stimulus size equal to the RF diameter. Error bars: s.d. of the bootstrapped distributions. *Dots:* individual MUs. **(I)** Scatter plot of percent change in Fano-factor evoked by a stimulus with diameter twice the RF diameter relative to the Fano-factor evoked by a stimulus matched to the RF diameter vs. suppression index (see Methods). *Color dots* identify units in different layers, and the *different symbols* show data from two different animals, as indicated. *Lines* are regression lines fitted to the individual layer data. **(J)** Scatter plot of percent change in Fano-factor evoked by a stimulus with diameter equal to the *per-neuron* RF-surround diameter relative to the Fano-factor evoked by a stimulus matched to the RF diameter vs. suppression index. Other conventions as in (I). **(K)** Percent change in Fano-factor evoked by a 26° diameter stimulus relative to the Fano-factor evoked by a stimulus matched to the RF diameter vs. suppression index. Other conventions as in (I).

Figure 3. Amplification of cortical response variability by small visual stimuli. (A) Three example MUs showing stimulus evoked increases in firing-rate and Fano-factor relative to baseline for small stimuli. **Top:** spike-rasters. **Middle:** PSTH of firing rate. *Dashed line:* baseline firing rate. **Bottom:** PSTH of Fano-factor. *Dashed line:* baseline Fano-factor. **(B)** Population-averaged time course of Fano-factor (*red*) and firing-rate (*black*) in SG **(Left),** G **(Middle),** and IG **(Right)**

layers computed at two stimulus diameters (**Top:** 0.1°, **Bottom:** 0.8°). Both the Fano-factor and firing rate were normalized to the pre-stimulus baseline of each unit before averaging. **(C)** Median stimulus diameter evoking the largest magnitude increase in Fano-factor, normalized to the RF diameter of the recorded MUs, for different layers. Error bars: s.d. of the bootstrapped distributions. *Dots* here and in (D-E)*:* individual MU data. **(D)** Median difference in Fano-factor (Fano-factor at the stimulus diameter causing the largest change in Fano-factor minus the baseline Fano-factor) ± s.d. of the bootstrapped distributions at max quenching (*gray*) and max amplification (*white*) for different layers. **(E)** Mean baseline Fano-factor for amplifier (*green*) and quencher (*yellow*) MUs. Error bars: s.e.m.

Figure 4. Size tuning of shared variance across V1 layers: example penetration. (A) Left: raster plots showing the spike times of four simultaneously recorded SG MUs, across several trials, in response to 0.1° (Top), 0.5° (Middle), and 26° (Bottom) diameter gratings. The responses of all 4 neurons in a single trial are shown between two consecutive horizontal lines. Horizontal lines separate different trials. **Right:** Network covariance matrices estimated with a single-factor factor analysis for each of the same 3 different stimulus diameters. The diagonal of the network covariance matrix holds the shared variance for each recorded MU. **Bottom:** Shared variance as a function of stimulus diameter. The *red markers* show mean±s.e.m. of the shared variance computed for the SG MU population recorded in this example penetration (n=4). The gray curves show the data for the four individual MUs. **(B,C)** same as in (A), but for G (n=3) and IG (n=7) layer MUs.

Figure 5. Size tuning of shared variance across V1 layers. (A) Top: Size tuning of shared variance (*red*) and firing rate (*black*) averaged over the population of SG (Left), G (Middle) and IG (Right) MU. *Solid lines*: fits to the data. *Dashed lines*: baseline shared variance (*red)* and firing rate (*black*), measured prior to stimulus onset. Error bars are: s.d. of the bootstrapped shared variance distribution (*red*) or s.e.m. (*black*). **Bottom:** Mean firing rate (*black*) and mean shared variance (*red*) as a function of normalized stimulus diameter, averaged over the population of recorded MUs separately for the different layers (SG, n=31 units; G, n=15; IG, n=36). The stimulus diameter was normalized to the RF diameter. **(B) Left:** RF-normalized shared variance averaged over the population at six different stimulus diameters (as indicated); shared variance values at specific stimulus sizes were extracted from functions fitted to the size-tuning data (see Methods).

Error bars: s.d. of the bootstrap distribution. **Right:** Box plots of normalized shared variance for MUs in SG, G, and IG layers at the same six stimulus diameters as shown in the left panel. *Dots*: shared variance values for individual MUs; *red horizontal lines*: medians. The extent of the box marks the quartiles of the data distribution, and the whiskers mark the width of the entire distribution, save for data points that are considered outliers because they are outside 1.5 times the inter-quartile range. **(C)** Median percent change in shared variance relative to baseline induced by a stimulus matched in size to the RF diameter for the different layers. *Dots here and in (D-F):* individual data points. Error bars: standard deviation of the bootstrapped distribution of medians. *Black and white dots* indicate data from different animals. **(D)** Median percent change in shared variance relative to a stimulus matched in size to the RF induced by a stimulus matched in size to twice the RF diameter (i.e. near surround) for the different layers. Other conventions as in panel C. **(E)** Median percent change in shared variance induced by a stimulus matched in size to the *per-neuron* surround diameter, relative to shared variance induced by a stimulus with diameter equal to the RF diameter, for the different layers. **(F)** Median percent change in shared variance induced by a 26° diameter stimulus relative to the shared variance evoked by a stimulus matched to the RF diameter, for different layers. **(G)** Median stimulus diameter at the smallest shared variance value (i.e. at max quenching), normalized to the RF diameter of the recorded MUs, for different layers. Error bars: 68% bootstrapped confidence interval of the median (can be asymmetric but otherwise corresponds to bootstrapped standard error). Other conventions as in panel (C). **(H)** Median stimulus diameter at the largest shared variance value in the RF surround (i.e. at max quenching), normalized to the RF diameter of the recorded MUs, for different layers. By construction of the analysis, the smallest possible value is 1. Conventions as in panel (G).

SUPPLEMENTARY METHODS

Mean-matched Fano-factor analysis

To ensure that the stimulus size-dependent modulation of variability was not a simple consequence of firing-rate modulation, we performed a mean-matched analysis (Mitchell et al., 2009; Churchland et al., 2010). First, for each time step of the analysis, the firing-rates of the recorded MUs were binned separately for the conditions being compared. Second, neurons were randomly removed from the bin containing the larger number of MUs, until the bin had an equal number of MUs for both stimulus conditions. This procedure was repeated for all time steps and firing-rate bins until the number of MUs in each firing-rate bin was equal across the conditions to be mean matched. Finally, Fano-factors for the remaining MUs were computed as described for the main analysis. To compute bootstrapped errors and statistics, this procedure was repeated 9999 times. For statistics, the resulting mean-matched PSTHs were averaged over time before computing the relevant statistics.

Single-unit analysis

To analyze the responses of spike-sorted SUs, the voltage traces (sampled at 30 kHz) of each channel were first high-pass filtered at 300Hz and then spikes were detected and clustered using Kilosort (Pachitariu et al., 2016). The clusters were manually refined using the graphical user interface Phy. We accepted units with signal-to-noise ratio (SNR) above 2.5 at the contact with the maximum spike amplitude. SNR is commonly used as a SU quality measure for electrode arrays recordings (Guillory and Normann, 1999), and similar SNR thresholds have been used in previous studies on cortical response variability (Rosenbaum et al., 2017).

Mean-matched Factor analysis

To mean-match the shared variability data, we first estimated shared variability for all neurons as described in the Results and Methods. Next, mean-matching of firing-rates was performed in the same way as described above for the mean-matching Fano-factor analysis. Finally, for the units

that survived mean-matching, shared variability was averaged and plotted as shown in **Figure 5-figure supplement 1.**

SUPPLEMENTARY RESULTS

Mean-matched Fano-factor analysis

In all layers, the mean matched Fano-factor analysis showed a statistically significant decrease in Fano-factor for a stimulus diameter matched to the RF size, evoking a higher mean spike count, relative to a 0.1-0.2° diameter stimulus (mean±bootstrapped 99% CI of the mean matched Fano-factor PSTH at 0.1-0.2° vs. RF stimulus diameter: SG, 2.41±0.06 vs. 1.83±0.05, p < 0.0001; G, 1.58±0.05 vs 1.39±0.06, p < 0.0001; IG, 1.90±0.04 vs 1.75±0.04, p < 0.0001; first and fifth columns in **Fig. 2- figure supplement 2A-C**).

For the SG layers, the mean-matched Fano-factor showed a significant increase, relative to a stimulus matched to the RF diameter, for all stimuli extending into the RF surround (**Fig. 2-figure supplement 2A**; mean±bootstrapped 99% CI of mean-matched Fano-factor at RF vs. 2xRF: 1.87±(0.05, 0.06) vs. 1.95±(0.06, 0.06); RF vs. 4xRF: 1.94±(0.07, 0.07) vs. 2.36±(0.07, 0.06); RF vs. 26° stimulus 1.65±(0.06, 0.09); p < 0.0001, bootstrap test for the difference in mean, with the null-hypothesis that the samples come from the same distribution).

The converse was true for G and IG layers, where Fano-factor showed a significant decrease, relative to a stimulus matched to the RF diameter, for stimuli extending into the RF surround (**Fig. 2- figure supplement 2B-C; G**: RF vs. 2xRF 1.06±(0.04, 0.05) vs. 1.01±(0.03, 0.03) p=0.003, RF vs. 4xRF 1.17±(0.05, 0.08) vs. 1.17±(0.03, 0.04) p=0.261, and RF vs. 26° diameter 1.35±(0.09, 0.11) vs. 1.16±(0.05 0.05) p=0.008; IG: RF vs. 2xRF 1.47±(0.03, 0.04) vs. 1.27±(0.03, 0.03) p<0.0001, RF vs. 4xRF 1.50±(0.03, 0.03) vs. 1.23±(0.02, 0.03) p<0.0001, and RF vs. 26° stimulus diameter 1.55±(0.03, 0.04) vs. 1.19±(0.03 0.03) p<0.0001).

Single unit analysis

We replicated the main analyses of this study for spike sorted SUs. Our SU sample was smaller than our MU sample, and consisted of 35 SG, 24 IG and 1 G layer SUs. As we had just one G layer

unit, we did not perform this analysis on G layer units, as meaningful statistical analyses could not be performed.

Individual SUs showed a similar variety of size tuning curves as the MUs (**Fig. 2-figure supplement 3A**). Similar to the MUs, for the majority (81% for SG and 52% for IG) of SUs, Fano-factor decreased as the stimulus diameter was increased to fill the RF (e.g. SG units # 44, 9, and IG units # 5, and 82).

Similar to the MUs, surround stimulation affected Fano-factor in three distinct ways: in all layers, in response to near or far surround stimulation, individual SUs could show increases, decreases, or no change in Fano-factor relative to its value for a stimulus matched to the RF, but the proportion of SUs showing each type of behavior varied somewhat between layers. To quantify this observation, similar to the MU analysis in **Fig. 2B**, we fitted functions to the individual SU Fano-factor size tuning curves and extracted from the fitted curves the Fano-factor measured at different stimulus sizes (**Fig. 2- figure supplement 3B**). We removed from this analysis 7 SG, and 8 IG SUs whose Fano-factor tuning curve was noisy and essentially flat. Thus, this analysis was performed on a total of 28 SG and 17 IG SUs. In both SG and IG layers, Fano-factor slightly decreased as the stimulus diameter was increased to 2x RF diameter (mean normalized Fano-factor ± bootstrap s.e., t-test on log-transformed data, RF vs. 2RF SG: 1.0±0 vs 0.93±0.03, p=0.03, IG: 1.0±0 vs 0.91±0.06, p=0.009). For larger stimuli, involving the far surround, in the IG layers Fano-factor plateaued to its value for near surround stimuli, whereas in the SG layers it increased back to larger values at the largest stimulus diameter (26°).

In both SG and IG layers, the population median stimulus diameter that evoked the lowest Fano-factor value (max quenching) in SUs was approximately twice the size of the RF (the near surround; **Fig. 2- figure supplement 3C**). The median (± bootstrapped s.e) stimulus diameter at lowest Fano-factor value normalized to the RF diameter was 2.6±1.5 in SG, and 2.5±1.8 in IG layers. However, there was considerable unit-to-unit variability in the stimulus diameter evoking the lowest Fano-factor value, as demonstrated by the individual data points in **Fig. 2-figure supplement 3C**; while the lowest Fano-factor value was often measured for a stimulus that extended into the RF surround, in a considerable proportion of SUs, the smallest Fano-factor was measured for a stimulus equal to, or smaller than, the RF. **Fig. 2-figure supplement 3D** shows the normalized stimulus diameter that evoked the highest Fano-factor. For this analysis, stimulus diameters equal to, or larger than, the RF were included. In SG layers, the median (± bootstrapped

s.e.) normalized stimulus diameter at the highest Fano-factor was 2.9±1.2, while in IG layers it was 1.1±1.2. Thus, similar to the MU data, in SG layers, far surround stimulation increased Fano-factor relative to Fano-factor for a stimulus in the RF, whereas it had no effect in IG layers.

Mean-matched Factor analysis

Mean-matched shared variance analysis produced similar results to the non-mean-matched analysis (**Fig. 5-figure supplement 1**). In all layers, the shared component of variability decreased when the stimulus diameter was increased from 0.1° to a size matching the RF diameter (0.1° vs RF mean±s.e.m., SG: 0.73±0.22 vs 0.25±0.09, G: 0.79±0.17 vs 0.15±0.03, IG: 0.53±0.17 vs 0.25±0.05, $p < 0.03$). Near surround stimulation (2xRF) had no significant effect on shared variance in any layer ($p > 0.06$). Stimulating the far surround had opposite effects on shared variability in SG and G layers compared to IG layers. In SG and G layers, increasing the stimulus diameter beyond the RF increased shared variance. In both layers, the shared variance was significantly higher when the stimulus diameter was 26° (but not when it was 4xRF) compared to when it matched the RF diameter (RF vs. 4xRF mean±s.e.m, SG: 0.20±0.05 vs. 0.37±0.16, $p = 0.09$; G: 0.11±0.02 vs. 0.17±0.03, $p = 0.10$; RF vs 26° mean±s.e.m. SG: 0.13±0.04 vs 0.61±0.21, G: 0.09±0.02 vs 0.19±0.04, $p < 0.03$). In contrast, far surround stimulation did not affect the shared variance in IG layers (RF vs. 4xRF mean±s.e.m.: 0.22±0.04 vs. 0.16±0.02 $p = 0.09$; RF vs 26° mean±s.e.m. 0.23±0.05 vs 0.16±0.03, $p = 0.15$).

SUPPLEMENTARY FIGURE LEGENDS

Figure 2 - figure supplement 1. Size tuning of Fano-factor across penetrations. The different color lines mark data recorded in different penetrations, for each layer group. Top: non-normalized data. Bottom: Normalized data; Fano Factor and grating diameter are both normalized to their values at the RF diameter.

Figure 2 - figure supplement 2. Mean-matched Fano-factor analysis. **(A)** SG layers. **Left** four columns: population-averaged PSTHs of mean firing rate and bootstrapped standard error (Top two panels) and of Fano-factor and bootstrapped standard error (Bottom two panels) for two

different stimulus diameters (from left to right: 0.1-0.2° vs. RF diameter; RF diameter vs. 2xRF diameter, RF diameter vs. 4xRF diameter, and RF diameter vs. 26°), after mean firing rate matching. **Right** four columns: population mean firing rate ± 99% bootstrapped confidence interval (CI) (Top) and mean Fano-factor ± 99% bootstrapped CI (Bottom) for the same two stimulus diameter comparisons, as indicated, after mean firing rate matching. **(B-C)** Same as in **(A)** but for G and IG layer MUs, respectively.

Figure 2 - figure supplement 3. Results for spike-sorted single-units. **(A)** Representative SG and IG SUs. **Top and Middle**: raster plots measured at two stimulus diameters, 0.8° (Top) and 26° (Middle). **Bottom:** mean firing-rate (*black*) and Fano-factor (*red*) as a function of stimulus diameter. *Solid lines*: fits to the data. *Dashed lines*: baseline Fano-factor (*red)* and firing rate (*black*), measured prior to stimulus onset. The error bars are s.e.m. for the firing-rate and bootstrapped s.e. for the Fano-factor. **(B)** **Left:** Mean normalized (to the RF diameter) Fano-factor for several stimulus diameters, as indicated, shown separately for SG and IG layers. Error bars: s.d. of the bootstrap distribution. **Right:** Box plots of normalized Fano-factor for SUs in SG and IG layers at the same six stimulus diameters as shown in the left panel. *Dots*: Fano-factor values for individual SUs; *red horizontal lines*: medians. **(C)** Median stimulus diameter at the smallest Fano-factor value (or max quenching), normalized to the RF diameter of the recorded SUs, for different layers. Error bars: s.d. of the bootstrapped distributions. *Dots:* individual SUs. **(D)** Median surround stimulus diameter at the highest Fano-factor value, normalized to the RF diameter. Error bars: s.d. of the bootstrapped distributions. *Dots:* individual SUs.

Figure 3 - figure supplement 1. Variability amplification is not due to eye movements. **(A)** Raster plots recorded across the linear electrode array in an example penetration (MK374-P2) in which a 0.6° stimulus (lasting 500ms) caused variability amplification in some units (same penetration and condition as in the left column of **Fig. 3A**). Each panel shows responses across the electrode array in a single trial. *Red*: SG layer units (n=7; a unit did not spike in this condition); *Black*: G layer units (n=3); *Cyan*: IG layer units (n=8).

Figure 5 - figure supplement 1. Mean-matched factor analysis. (A) SG layers. Population mean±s.e.m. firing rate (Top) and mean±s.e.m. shared variance (Bottom) for different stimulus

diameter comparisons, after mean firing rate matching. RF: stimulus matching the RF diameter. **(B,C)** Same as in (A) but for G and IG layer units, respectively.

Figure 1

Figure 2

Figure 3

Figure 4

Figure 5

Figure 2 - figure supplement 1

Size tuning of Fano-factor across penetrations. The different color lines mark data recorded in different penetrations, for each layer group. <u>Top:</u> Non-normalized data. <u>Bottom:</u> Normalized data; Fano factor and grating diameter are both normalized to their values at the RF diameter.

Figure 2 - figure supplement 2

Mean-matched Fano-factor analysis. (A) SG layers. **Left** four columns: population-averaged PSTHs of mean firing rate and bootstrapped standard error (Top two panels) and of Fano-factor and bootstrapped standard error (Bottom two panels) for two different stimulus diameters (from left to right: 0.1-0.2° vs. RF diameter; RF diameter vs. 2xRF diameter, RF diameter vs. 4xRF diameter, and RF diameter vs. 26°), after mean firing rate matching. **Right** four columns: population mean firing rate ± 99% bootstrapped confidence interval (CI) (Top) and mean Fano-factor ± 99% bootstrapped CI (Bottom) for the same two stimulus diameter comparisons, as indicated, aftermean firing rate matching. **(B-C)** Same as in (A) but for G and IG layerMUs, respectively

Figure 2 - figure supplement 3

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Figure 5 - figure supplement 1

Mean-matched factor analysis. (A) SG layers. Population mean±s.e.m. firing rate (Top) and mean±s.e.m. shared variance (Bottom) for different stimulus diameter comparisons, after mean firing rate matching. RF: stimulus matching the RF diameter. (**B,C**) Same as in (A) but for G and IG layer units, respectively.