Leading and Following: Noise Differently Affects Semantic and Acoustic Processing during Naturalistic Speech Comprehension

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Abstract

Despite the distortion of speech signals caused by unavoidable noise in daily life, our ability to comprehend speech in noisy environments is relatively stable. However, the neural mechanisms underlying reliable speech-in-noise comprehension remain to be elucidated. The present study investigated the neural tracking of acoustic and semantic speech information during noisy naturalistic speech comprehension. Participants listened to narrative audio recordings mixed with spectrally matched stationary noise at three signal-to-ratio (SNR) levels (no noise, 3 dB, -3 dB), and 60-channel electroencephalography (EEG) signals were recorded. A temporal response function (TRF) method was employed to derive event-related-like responses to the continuous speech stream at both the acoustic and the semantic levels. Whereas the amplitude envelope of the naturalistic speech was taken as the acoustic feature, word entropy and word surprisal were extracted via the natural language processing method as two semantic features. Theta-band frontocentral TRF responses to the acoustic feature were observed at around 400 ms following speech fluctuation onset over all three SNR levels, and the response latencies were more delayed with increasing noise. Delta-band frontal TRF responses to the semantic feature of word entropy were observed at around 200 to 600 ms leading to speech fluctuation onset over all three SNR levels. The response latencies became more leading with increasing noise and were correlated with comprehension performance and perceived speech intelligibility. While the following responses to speech acoustics were consistent with previous studies, our study revealed the robustness of leading responses to speech semantics, which suggests a possible predictive mechanism at the semantic level for maintaining reliable speech comprehension in noisy environments.

Keywords: speech-in-noise comprehension, semantic processing, neural tracking, temporal response function, EEG

Highlights

1. Leading responses were observed in the semantic-level neural tracking, with more leading latencies as

noise increased.

2. Following responses were observed in the acoustic-level neural tracking, with more delayed latencies as

noise increased.

3. Semantic-level neural tracking is correlated with comprehension performance and perceived

intelligibility.

4. Distinct frequency bands were involved in speech semantic and acoustic processing.

1 Introduction

Noise is an inevitable part of daily life, from car horns on the streets to background music at parties, and it presents a significant challenge to verbal communication. Reliable speech comprehension in noisy environments is crucial in various situations such as education or emergency service. Despite the distortion of auditory information, individuals with normal hearing can comprehend speech with ease. Understanding the adaptive neural mechanisms that enable robust speech-in-noise comprehension is essential for clinical intervention for hearing/language-impaired groups and for developing hearing-aid techniques.

Neurophysiological studies have revealed important insights into how noise affects speech processing. Using the event-related techniques, cortical auditory evoked potentials (CAEP) elicited by auditory and speech stimuli have been found to show delayed latencies and reduced amplitudes under adverse conditions, including the early component P1-N1-P2 complex related to primary sound processing (Billings et al., 2009, 2011), and the later components such as the N2 component related to phonological analysis (Billings et al., 2009; Martin & Stapells, 2005; Tomé et al., 2015; Whiting et al., 1998) and the P3 component related to speech discrimination (Kaplan-Neeman et al., 2006; Koerner et al., 2017; Martin & Stapells, 2005; Whiting et al., 1998). In recent years, studies have focused more on the neural tracking of continuous speeches. i.e., the alignment between neural activities and the quasi-rhythmic fluctuations of continuous speech (see reviews, Brodbeck & Simon, 2020; Ding & Simon, 2014; Giraud & Poeppel, 2012; Lakatos et al., 2019; Obleser & Kayser, 2019). Specific temporal dynamics of neural tracking can be described via system identification methods such as the temporal response function (TRF; Crosse et al., 2016, 2021) by relating neural signals with speech features such as acoustic envelope. Neural tracking has been found to remain stable under mild and moderate noise, and it is regarded as an essential tool for segregating speech from the noisy background (Ding & Simon, 2013). Nevertheless, the TRF-based studies have also reported delayed latencies and/or reduced amplitudes of the neural tracking in noisy conditions (Gillis, Decruy, et al., 2022; Mirkovic et al., 2019; Muncke et al., 2022; Zou et al., 2019), similar to previous event-related studies. These results suggest an impaired acoustic processing efficiency in noisy environments (Gillis, Decruy, et al., 2022; Kaplan-Neeman et al., 2006). In addition to auditory processing, semantic processing also plays a vital role in speech-in-noise comprehension and has been paid substantial emphasis.

Semantic processing could be a crucial factor in robust speech comprehension against noisy

environments. Numerous research has shown that coherent semantic context enabling anticipating

upcoming stimuli contributes to an effective understanding of degraded speech (Miller et al., 1951; Obleser

& Kotz, 2010, 2011; Sohoglu et al., 2012; Zekveld et al., 2011). For example, Miller et al. (1951) found

that words in coherent sentences had higher intelligibility compared with the same words in unrelated word

lists during speech-in-noise comprehension. Regarding the influence of noise on semantic processing, such

as the N400 component (Kutas & Federmeier, 2011; Kutas & Hillyard, 1984), several studies have reported

robust or increased amplitude of N400 under mild degradation, which might be related to additional

cognitive effort (Jamison et al., 2016; Romei et al., 2011; Zendel et al., 2015), while other studies reported

reduced/delayed N400 for degraded speech, which might be related to damaged signal quality (Aydelott et

al., 2006; Connolly et al., 1992; Daltrozzo et al., 2012; Obleser & Kotz, 2011; Strauß et al., 2013). These

mixed results provided valuable information on the complex relationship between noise and semantic

processing. Moreover, it was discovered that semantic processing includes early responses before the onset

of the stimulus, which was considered to be associated with semantic prediction (Grisoni et al., 2017, 2021;

Pulvermüller & Grisoni, 2020). Nevertheless, it is still unknown how this pre-onset response is modulated

by noise at various signal-to-ratios (SNRs). These inconsistent results and inadequate explorations of noise

effect on semantic processing may be due to limitations inherent in the event-related design. This design

typically uses highly-controlled and short-duration speech units, such as individual words (e.g., Romei et

al., 2011) or disconnected sentences (e.g., Strauß et al., 2013), which only contain limited

semantic/contextual information.

The recent rise of the naturalistic speech paradigm is expected to expand our knowledge of the neural

mechanisms of semantic processing during speech-in-noise comprehension (Z. Li & Zhang, 2023).

Compared to the highly-controlled and short-duration speech units, continuous naturalistic speech stimuli

provide a better resemblance to our daily communications because of a longer duration, more flexible

content, and less deliberate semantic violations (Alday, 2019; Alexandrou et al., 2020; Hartley & Poeppel,

2020; Sonkusare et al., 2019; Willems et al., 2020; Wöstmann et al., 2017). Most of all, the continuous

naturalistic speech stimuli provide rich context-based semantic information (Alday, 2019; Alexandrou et

al., 2020; Hamilton & Huth, 2020; Sonkusare et al., 2019), which is indispensable for semantic prediction

and reliable speech comprehension in chaotic daily environments. In addition, via state-of-art

computational linguistic models, the semantic information of naturalistic speech can be quantified, and the

semantic-level neural tracking can be directly measured (Broderick et al., 2018, 2019, 2021; Gillis et al.,

2021; Koskinen et al., 2020; Mesik et al., 2021; Weissbart et al., 2020), presenting a powerful tool to

investigating how semantic processing is affected by noise at different SNRs.

The two frequently adopted semantic features in speech-related neuroscience research are entropy and

surprisal derived from information theory (Brodbeck et al., 2022; Donhauser & Baillet, 2020; Goldstein et

al., 2022; Heilbron et al., 2022), which respectively measures the semantic uncertainty of the upcoming

stimuli and the unexpectedness of the current stimulus (Pickering & Gambi, 2018; Willems et al., 2016).

The word surprisal was found to be associated with the superior temporal gyrus and inferior frontal sulcus,

etc. (Willems et al., 2016), and is linked to an N400-like neural response, i.e., negativity at around 400 ms

within the central-parietal electrodes (Broderick et al., 2021; Gillis et al., 2021; Heilbron et al., 2022). The

word entropy was associated with neural activities within the left ventral premotor cortex, left middle

frontal gyrus and right inferior frontal gyrus, etc. (Willems et al., 2016). Furthermore, Goldstein et al. (2022)

derived word entropy from deep language models (GPT-2) and correlated them with electrocorticography

(ECoG) signals. The results indicated that entropy was related to neural activities in the left-lateralized

channels at several hundred milliseconds before the word onset. This pre-onset response is consistent with

the semantic prediction potential (SPP) in event-related studies as a direct neural signature for semantic

prediction (Grisoni et al., 2021; Pulvermüller & Grisoni, 2020). A recent study by Yasmin et al. (2023)

discovered that the N400-like response in semantic-level neural tracking remained robust under mild and

moderate noise conditions and declined abruptly at the high-noise level (SNR = -3 dB). However, the noise

effect on the pre-onset response in semantic-level neural tracking is still unexplored.

The current study aimed to investigate the neural mechanisms of speech-in-noise comprehension by

simultaneously focusing on both the acoustic and semantic levels as well as both the pre-onset and the post-

onset stages. A naturalistic speech comprehension paradigm was employed, as the naturalistic speech

stimuli were expected to provide better ecological validity and contextual information (Alday, 2019;

Sonkusare et al., 2019). 60-channel EEGs were recorded while the participants listened to spoken narratives

at three SNRs (no noise, 3 dB, -3 dB). Following previous studies, the amplitude envelopes of the speech

stimuli were extracted as the acoustic feature (Di Liberto et al., 2015; O'Sullivan et al., 2015). Two typical

semantic features were calculated by a Chinese NLP model, i.e., word entropy and word surprisal (Gillis et

al., 2021; Weissbart et al., 2020; Willems et al., 2016; Koskinen et al., 2020; Mesik et al., 2021; Broderick

et al., 2021). The neural responses to the acoustic and semantic features were estimated using the TRF

method (Crosse et al., 2016), which yields the spatiotemporal dynamics of how our brain tracks these

features in naturalistic speeches. The pre-onset and post-onset responses in the current study were defined

as significant TRF responses with negative and positive time lags, respectively. Especially, we conducted

TRF analyses and detected significant TRF responses separately at different SNR levels to capture all

potential neural signatures. We hypothesize that the acoustic-level TRF could be related to delayed peak

latencies or reduced amplitudes under noisy conditions as in previous studies (Gillis, Decruy, et al., 2022;

Mirkovic et al., 2019; Muncke et al., 2022; Zou et al., 2019). As for the semantic-level TRF, we hypothesize

that both the pre-onset and post-onset response could show resilience against noise (Yasmin et al., 2023).

By exploring the pre-onset and post-onset temporal dynamics of low- and high-level processing, this study

hopes to gain a more complete overview of the noise effect on neural processing during naturalistic speech

comprehension.

2 Methods

2.1 Participants

Twenty college students (10 females, ages ranging from 19 to 28 years old) participated in the study. The sample size was determined to be sufficient by reference to previous TRF-based studies on the human speech processing (e.g., Broderick et al., 2018; Di Liberto et al., 2015). One male participant was excluded due to technical problems during data recording. The data of the remaining nineteen participants (age: mean $\pm$ SD = 21.79 $\pm$ 1.99) were included in the subsequent analyses. All participants were native Chinese speakers, right-handed, with normal hearing and normal or corrected-to-normal vision by self-report. The study was conducted in accordance with the Declaration of Helsinki and was approved by the local Ethics Committee of Tsinghua University. Written informed consent was obtained from all participants.

2.2 Materials

Thirty narrative audio recordings from our previous studies (Z. Li et al., 2021, 2022) were used as stimuli. These audio recordings were recorded from six native Chinese speakers with professional training in broadcasting. The participants were unfamiliar with the content of these narrative audio recordings, which were about speakers' personal experiences on daily-life topics adapted from the National Mandarin Proficiency Test. Each narrative audio recording lasted for around 90 s and was recorded by a regular microphone at a sampling rate of 44,100 Hz in a sound-attenuated room.

These speech stimuli were further processed into three versions at three different SNR levels: no-noise (NN), low-noise (SNR = 3 dB), and high-noise (SNR = -3 dB), where speech intensity percentage was 100%, 60%, and 40%, respectively. This procedure was achieved by adding spectrally matched stationary noise, which was generated based on a 50th-order linear predictive coding (LPC) model estimated from the original speech recording (Broderick et al., 2018). The SNR levels were selected following previous studies (Ding & Simon, 2013), and were produced by varying the noise intensity while keeping the intensity of original speech (measured by its root mean square) constant (Ding & Simon, 2013).

For each narrative audio recording, two four-choice questions were prepared by the experimenters to assess one's speech comprehension performance. These questions and the corresponding choices were targeted at detailed narrative contents that would demand significant attentional efforts. For instance, one

question following a narrative audio recording about one's major was, "What is the speaker's most likely

major as a graduate student? (说话人的研究生专业最可能是什么？)" and the four choices were 1) Social

science, 2) International politics, 3) Pedagogy and 4) Psychology (1. 社会科学, 2. 国际政治, 3. 教育学 and

4. 心理学).

2.3 Procedure

Before the start of the experiment, the participants had one practice trial to get familiar with the

procedure, with an additional narrative audio recording at the no-noise level not used in the formal

experiment. The formal experiment consisted of 30 trials, with 10 trials per SNR level. In each trial, the

participants listened to narrative audio recordings at one of the three SNR levels. The participants were

required to maintain visual fixation on a fixation cross displayed on the computer screen in front of them

and to minimize eye blinks and all other motor activities during listening. The order of the narrative audio

recordings and their assigned SNR levels was randomized for each participant.

After each trial, the participants were instructed to answer two four-choice questions about the content

of the narrative audio recording using the computer keyboard. The averaged accuracies across all trials

(separately for each SNR level) were used to reflect the participants' comprehension performance. After

completing these questions, the participants were instructed to rate the perceived clarity and intelligibility

of the narrative audio recording on a 100-point rating scale and rested for at least 5 s before moving on to

the next trial. No feedback was given to the participants about their comprehension performance during the

experiment.

The experimental procedure was programmed in MATLAB using the Psychophysics Toolbox 3.0

(Brainard, 1997). The speech stimuli were delivered to listeners seated in a sound-attenuated room via an

air-tube earphone (Etymotic ER2, Etymotic Research, Elk Grove Village, IL, USA) to avoid environmental

noise and equipment electromagnetic interference. The volume of the audio stimuli was adjusted

individually for each participant to a comfortable level, and it was kept consistent across trials. The

experimental procedure is illustrated in Figure 1.

Figure 1. Experimental procedure. The participants listened to 30 naturalistic narrative audio recordings
which each lasted around 90 s. These audio recordings were mixed with three levels of spectrally matched
stationary noise: no-noise (NN), low-noise (SNR = 3 dB), and high-noise (SNR = -3 dB). The 60-channel
EEG signals were recorded during listening. After listening to each narrative audio recording, the
participants were required to complete a comprehension test and report the clarity and intelligibility rating.
In the comprehension test, two four-choice questions per audio recording based on the narrative content
were used.

2.4 EEG recording and preprocessing

EEG signals were recorded from 60 channels with a NeuroScan amplifier (SynAmp II, NeuroScan,

Compumedics, USA) at a sampling rate of 1000 Hz. Electrodes were positioned according to the

international 10–20 system, including FP1/2, FPZ, AF3/4, F7/8, F5/6, F3/4, F1/2, FZ, FT7/8, FC5/6, FC3/4,

FC1/2, FCZ, T7/8, C5/6, C3/4, C1/2, CZ, TP7/8, CP5/6, CP3/4, CP1/2, CPZ, P7/8, P5/6, P3/4, P1/2, PZ,

PO7/8, PO5/6, PO3/4, POZ, Oz, O1/2, referenced to an electrode between CZ and CPZ with a forehead

ground at FZ. Electrode impedances were kept below 10 kOhm for all electrodes throughout the experiment.

The recorded EEG data were first notch filtered to remove the 50 Hz powerline noise. Independent

Component Analysis (ICA) was performed to remove artifacts such as eye blinks and eye movements based

on visual inspection. Around 4–12 independent components (ICs; mean = 6.6) were removed per participant.

The remaining ICs were then back-projected onto the scalp EEG channels to reconstruct the artifact-free

EEG signals. The EEG signals were then re-referenced to the average of all scalp channels and

downsampled to 128 Hz. Afterward, EEG signals were filtered into the delta (1–4 Hz) and theta (4–8 Hz)

bands, which have been previously reported to be important for speech neural tracking (Ding et al., 2014;

Etard & Reichenbach, 2019; Keitel et al., 2017; Koskinen et al., 2020; J. Li et al., 2023; Peelle et al., 2013).

For comprehensiveness, we also included the alpha (8–12 Hz) and beta (12–30 Hz) bands into analyses.

Causal FIR (Finite Impulse Response) filters were employed to ensure that the filtered EEG signals were

determined only by the current and previous data samples, which was important for the present study

focusing on the fine-grained time course, particularly considering the pre-onset neural responses (de

Cheveigné & Nelken, 2019).

These preprocessed EEG signals were segmented into 30 trials, from 5 to 90 s (duration = 85 s),

relative to the speech onsets of each trial to avoid possible onset and offset effects. All preprocessing was

conducted offline using MATLAB and the Fieldtrip toolbox (Oostenveld et al., 2011).

2.5 Feature extraction

Three types of features were extracted to represent the acoustic (amplitude envelope) and semantic

(word entropy, word surprisal) information for each narrative audio recording. An example of these speech

features is illustrated in Figure 2A.

Acoustic feature. The amplitude envelope for each narrative audio recording was calculated as the

absolute values after a Hilbert transform and then downsampled to the sampling rate of 128 Hz to match

that of the EEG signals.

Semantic features. Before feature extraction, the narrative audio recordings were converted to text by

Iflyrec software (Iflytek Co., Ltd, Hefei, Anhui) and then segmented into words based on the THU Lexical

Analyzer for Chinese (THULAC) toolbox (Sun et al., 2016).

Two semantic features, word entropy and word surprisal, were extracted. Word entropy measures the

uncertainty of predicting the upcoming word based on the context so far and was calculated as equation (1):

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$$Entropy(t) \ = \ - \sum_{w_{t+1}} P(w_{t+1}|w_1, \ldots, w_t) log P(w_{t+1}|w_1, \ldots, w_t) \tag{1}$$

244 Word surprisal measures how surprising the current word is given the previously encountered words and

245 was calculated as equation (2):

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$$Surprisal(t) \ = \ - log P(w_t|w_1, \ldots, w_{t-1}) \tag{2}$$

Where $w_1, ..., w_{t-1}$ are the existing word sequence and $P(w_t|w_1, ..., w_{t-1})$ is the conditional probability of

next word (Willems et al., 2016). These NLP calculations were conducted by ADAM, a widely accepted

Long-Short Term Memory (LSTM) Neural Network model (Kingma & Ba, 2015). The model was trained

on the corpora corpus of the People's Daily with 534,246 Chinese words. See Supplementary Table S1 for

more information about the model and Supplementary Table S2 for more information about the descriptive

statistics of semantic features.

After extracting the semantic features of each word, the word onset timings were estimated via Iflyrec

software. Impulses at the word onset time were manipulated with corresponding semantic feature values to

generate one-dimensional "semantic vectors" (e.g., Broderick et al., 2018; Gillis et al., 2021). The sampling

rate of the semantic vectors was 128 Hz to match the EEG signals.

Figure 2. Speech feature extraction and Temporal Response Function analyses. (A) Three types of speech

features were extracted, including one acoustic feature (amplitude envelope) and two semantic features

(word entropy and word surprisal). The two semantic features were derived from a computational linguistic

model and one-dimensional vectors were generated with impulses manipulated with semantic feature values

at the corresponding word onsets time. (B) Forward modeling. TRFs were extracted by regressing each of

the three types of speech features against the EEG signals separately. The significance of these TRFs was

estimated by comparing them with the corresponding control TRFs, which were modeled based on EEG

signals and shuffled speech features. The resulting spatiotemporal ranges were identified as regions of

interest (ROIs) and time lags of interest (TOIs). (C) Backward modeling. These three types of speech

features were separately reconstructed through backward TRF models, and the reconstruction accuracy

(Pearson's *r*) depicted the strength of neural tracking. Control backward models were constructed with EEG

signals and shuffled features.

2.6 Modeling of the stimulus-response relationship

The Temporal Response Function (TRF) modeling method based on ridge regression was adopted to

explore the relationship between the neural activities and the three types of stimulus features (Crosse et al.,

2016, 2021). Forward modeling was first used to illustrate the specific spatiotemporal response patterns

and identify key electrodes and time lags in TRF responses of the corresponding speech feature, and then

backward modeling was adopted to verify the possible contribution of these identified neural correlates

(e.g., Broderick et al., 2019; Etard & Reichenbach, 2019). The overall procedure of the modeling analyses

is shown in Figure 2B and 2C.

Forward modeling. With a forward modeling approach, we described neural response patterns to

different speech features by linear spatiotemporal filters called TRFs, which measure how neural signals

from different regions are modulated by stimulus features at different time lags (Crosse et al., 2016). The

estimated TRF together with the corresponding speech feature was used to predict the EEG responses from

each electrode. The prediction accuracy measured as the Pearson's correlation between the actual and

predicted EEG signals represents the performance of the forward model. The TRF, *w*, is measured by

equation (3):

$$w = (S^T S + \lambda I)^{-1} S^T r \tag{3}$$

Where *S* is the lagged time series of the stimulus features, *r* is the neural signals, and *I* is the identity

matrix. The time lags for forward modeling were chosen to cover a relatively broad time range, from -1000

to 1000 ms (Goldstein et al., 2022; J. Li et al., 2021, 2023). The λ is the regularization parameter used to

prevent overfitting and ranged between 0.1 and 1000 in steps of the powers of 10 empirically (Gillis, Van

Canneyt, et al., 2022). The cross-validation procedure was implemented in a leave-one-trial-out procedure

within each participant: each time, the model was trained based on 9 trials and tested on the left-out trial,

which was repeated for each of the 10 trials at three SNR levels separately. The λ value that produced the

highest prediction accuracy averaged across trials after cross-validation was selected as the regularization

parameter for all trials at a certain SNR level per participant. TRF amplitudes were further transformed into

z-scores before statistical analyses (Ding et al., 2014; Gillis et al., 2021; J. Li et al., 2021).

The statistical significance of the estimated TRFs was estimated by constructing control TRF models

(Weissbart et al., 2020). We built control models by constructing TRF models using shuffled stimulus

features and the EEG recordings in the same way as for the computation of the actual TRFs. The shuffled

amplitude envelope was constructed by randomly shuffling the feature value within a trial while keeping

the timing of the quiet fragments. The shuffled word entropy and word surprisal were constructed by

randomly shuffling the feature value within a trial while keeping the timing of impulses. Therefore the

speech features that described acoustic and linguistic word onsets were not altered and thus left no impact

on TRFs' significance (Weissbart et al., 2020). The shuffling was repeated 1,000 times and resulted in

1,000 control TRFs for a corresponding actual TRF.

A nonparametric cluster-based permutation test was applied to account for multiple comparisons

(Maris & Oostenveld, 2007). For each electrode-time bin in the actual and control TRFs, a one-sample t-

test was used to examine whether the TRF amplitudes significantly differed from 0. Then neighboring

electrode-time bins with an uncorrected p-value less than 0.01 were combined into clusters. The minimum

number of neighboring significant channels that was required for inclusion in a cluster was 2. For each

cluster, the sum of the t-statistics was obtained. A null distribution was created from the 1,000 control test

statistics, i.e., the maximum cluster-level t-statistics. The corrected p-value for each cluster was calculated

as the proportion of control test statistics greater than the actual cluster-level t-statistics. Clusters with p-

values below 0.05 were selected for further analyses. We implemented the same statistical analyses

procedure for each of the 18 TRFs (3 stimulus features $\times$ 2 frequency bands $\times$ 3 SNR levels). The EEG

electrodes and time lags from significant clusters were regarded as ROIs/TOIs. Then peaks were estimated

within these ROIs/TOIs, and the peak amplitudes and peak latencies were compared across different SNRs.

Backward modeling. With a backward modeling approach, we simultaneously took neural signals from

several electrodes to reconstruct stimulus features with a decoder. The reconstruction accuracy was

measured as the Pearson's correlation between the actual and reconstructed stimulus features. The decoder,

g, is calculated by equation (4), where R is the lagged time series of the EEG data. The reconstructed feature,

$\hat{s}(t)$, is calculated by equation (5) where n is the EEG electrodes, and τ is the time lags (Broderick et al.,

2019).

$$g = (R^T R + \lambda I)^{-1} R^T s \tag{4}$$

$$\hat{s}(t) = \sum_n \sum_\tau r_n(t + \tau) g_n(\tau) \tag{5}$$

Only the exact ROIs/TOIs from significant clusters found in the forward modeling were included in

the backward modeling. The EEG signals and stimulus features were downsampled to 64 Hz for better

computational efficiency. The same leave-one-trial-out cross-validation procedure as in the forward

modeling approach was conducted to obtain the optimal regularization parameter and calculate the

reconstruction accuracy. We also estimated the control decoders using the same shuffling methods in

forward modeling. The reconstruction accuracies from the 1,000 control decoders were averaged and

compared with the actual decoder via a one-tailed paired *t*-test, and the *p* values of clusters were corrected

via the false discovery rate (FDR) method (Benjamini & Hochberg, 1995).

In sum, the analyses of neural tracking followed two main steps. (1) We calculated the actual forward

model and control forward models and identified ROIs/TOIs according to clusters with significant

differences between them. (2) We estimated the reconstruction accuracy based on these ROIs/TOIs. This

procedure resulted in (1) the specific spatiotemporal TRF response pattern and (2) the strength of neural

tracking (reconstruction accuracy) for analyses.

Given that the neural signatures of speech processing could exhibit different spatiotemporal patterns

at various SNR levels (e.g., Bidelman & Howell, 2016; Billings et al., 2009; Strauß et al., 2013), we

conducted separate statistical tests for identifying significant clusters in the TRF responses at different SNR

levels, in order to capture all potentially significant results without missing anything.

We classified these significant clusters into two types based on their spatiotemporal dynamics: those

with largely overlapped spatiotemporal patterns across all SNR levels, which could represent a reliable

response across all SNR levels, and those with unique patterns at a certain SNR level, which might signify

distinct processing mechanisms under certain circumstances. This was achieved by visual inspection and

calculating a similarity index, which derived from the average of the temporal and spatial similarity. See

Supplementary Figure S2 for more information. The consistent clusters were compared to explore how the

commonly shared neural signature adapted to noise, while the unique clusters received less attention in

subsequent analyses. Linear-mixed effect (LME) models and Spearman's correlation was conducted to

examine the relationship between neural tracking and behavioral performance.

Before modeling, the three types of stimulus features across all trials and EEG signals across all

channels were z-scored as recommended to ensure consistent scaling (Crosse et al., 2016, 2021). Modeling

and analyses for different stimulus features were conducted independently. Considering we focused on the

neural tracking of underlying hierarchical information in speech rather than physical stimulus, we adopted

the same stimulus features of no-noise speech for the other two SNR levels (Ding & Simon, 2013; Fuglsang

et al., 2017). The forward and backward modeling was conducted in MATLAB using the Multivariate

Temporal Response Function (mTRF) toolbox (Crosse et al., 2016). The cluster-based permutation test was

conducted in the FieldTrip toolbox (Oostenveld et al., 2011). Other statistical analyses were conducted via

MATLAB functions and IBM SPSS Statistics software (IBM corp., 2019).

3 Results

3.1 Behavioral performance

The speech comprehension performance was measured as the averaged response accuracy of the four-choice questions and was found to be significantly different among the three SNR levels (rmANOVA, $F(2, 36) = 6.74$, $p = .003$). The speech comprehension performance was $95.26 \pm 1.05\%$, $90.79 \pm 2.10\%$, and $85.26 \pm 2.63\%$ (mean $\pm$ SE) at the no-noise level, low-noise level, and high-noise level, respectively. The comprehension performance at the high-noise level was significantly lower than that at the no-noise level (post-hoc t-test, $p = .006$, Bonferroni corrected). In addition, it should be noted that the comprehension performance was still well above chance level even at the high-noise level (one-tailed t-test, $t(18) = 22.88$, $p < .001$).

The subjective ratings of clarity and intelligibility showed a similar pattern with significant differences among the SNR levels (rmANOVA, $F(2, 36) = 148.32$ and 35.31, ps $< .001$). The normalized clarity rating scores were 0.94 ± 0.01, 0.66 ± 0.04, and 0.35 ± 0.04 (mean $\pm$ SE), and the normalized intelligibility rating scores were 0.93 ± 0.01, 0.88 ± 0.02, and 0.73 ± 0.03 (mean $\pm$ SE) at the no-noise, low-noise, and high-noise level, respectively. Post hoc t-tests revealed significant pairwise differences for all possible comparisons (ps $< .01$, Bonferroni corrected). The behavioral performance is illustrated in Figure 3. These results suggested that the effect of noise on speech comprehension and perception was effectively manipulated.

Figure 3. Behavioral results. Black dots indicate data points from each participant. Error bars denote the standard error. *: $p < .05$, **: $p < .01$, ***: $p < .001$.

3.2 Summary of all significant clusters in the acoustic- and semantic-level TRF responses

We summarized all significant clusters in the acoustic- and semantic-level TRF responses in Figure 4.

Significant clusters were only found in the delta/theta bands but not alpha/beta bands (see Supplementary

Figure S1 for more information). The specific time lags of TOIs of clusters were listed in Supplementary

Table S3-4. According to visual inspection and the similarity index (shown in Supplementary Figure S2),

these significant clusters were classified into responses that exhibited relative consistency across different

SNR levels, as well as distinctive response at a certain SNR level.

Clusters with largely overlapped spatiotemporal patterns across all SNR levels were found in theta-

band acoustic-level TRFs (i.e., A1, A2, A3) and delta-band entropy-based semantic-level TRFs (i.e., E1,

E2, E3). Detailed analyses of them are demonstrated in the section 3.3 and 3.4, respectively. Several clusters

with similar spatiotemporal patterns shared by certain SNR levels, such as the acoustic-level TRF response

within the occipital electrodes (i.e., A4 and A5) and the post-onset entropy-based semantic-level TRF

responses within the central electrodes (i.e., E5 and E6). Analyses of them are demonstrated in

Supplementary Figure S3 and S4. No further analysis was done for the other unique clusters at the no-noise

level. No significant TRF responses to word surprisal were found.

Figure 4. Significant clusters in TRF responses to (A) amplitude envelope, (B) word entropy, and (C) word surprisal at different SNR levels and frequency bands. Significant clusters are numbered A1−A5 and E1−E8. Clusters with similar spatiotemporal patterns are organized in the same row. ROIs of clusters are shown as black dots in the corresponding topography. The colored curves are the mean of TRFs averaged among ROIs across participants. The shaded areas denote the standard error of TRFs. The colored horizontal line below the TRF curve indicates the TOIs of the cluster. The *a* and *b* refer to clusters with the same ROIs but different TOIs. n.s.: no significant cluster was found.

3.3 Acoustic-level TRF responses with delayed latencies as noise increases

Significant acoustic-level TRF responses in the theta band were found at all SNR levels and showed a similar positivity within central electrodes at around 300~500 ms (i.e., A1, A2a, A3b), as demonstrated in Figure 5A. At the no-noise level, the TRF showed positivity in the central electrodes with a latency of around 400 ms (cluster-level $p < .01$). At the low-noise and high-noise levels, the TRF showed similar positivity in the central electrodes with a latency of around 430 (cluster-level $p < .01$) and 440 ms (cluster-level $p < .01$). We estimated the peak amplitude and peak latency for the positive peak at each SNR level. The peak latencies were significantly different among the three SNR levels (rmANOVA, $F(2, 36) = 21.42$, $p < .001$), and post-hoc *t*-tests revealed significantly delayed peak latencies as noise increased ($ps < .05$, Bonferroni corrected), as shown in Figure 5C. No significant differences were found in the peak amplitudes (rmANOVA, $F(2, 36) = 0.64$, $p = .535$).

The reconstruction accuracies from the corresponding ROIs/TOIs were significantly higher in the

actual decoders than in the control decoders ($ps < .01$, FDR corrected, Figure 5B). Comparing the

reconstruction accuracies revealed significant differences among the three SNR levels (rmANOVA, $F(2,$

$36) = 6.19$, $p = .010$ with Greenhouse-Geisser correction), and post-hoc t-tests revealed significantly

weakened neural tracking at the high-noise level compared with the no-noise level and the low-noise level

($ps < .05$, Bonferroni corrected, Figure 5C).

Figure 5. Acoustic-level TRF responses in the theta band at different SNR levels. (A) The bold curves in

different shades of red are the mean of TRFs averaged among ROIs across participants at the three SNR

levels. The grey curves are TRFs averaged among the ROIs of each participant. The colored horizontal line

at the bottom of each plot indicates TOIs over which TRFs differed significantly from the control models.

Dots in the corresponding topographies depicted the ROIs. (B) Reconstruction accuracy calculated from

the ROIs/TOIs in (A). AM means actual models. CM means control models. (C) Noise effect on the peak

amplitude, peak latency, and reconstruction accuracy. Grey dots indicate data points from each participant.

Error bars denote the standard error. n.s.: not significant, *: $p < .05$, **: $p < .01$, ***: $p < .001$.

3.4 Semantic-level TRF responses with earlier latencies as noise increases

Significant semantic-level TRF responses to word entropy in the delta band were found at all SNR

levels. They showed similar negativity at around 200~600 ms leading to speech fluctuation onset, as

demonstrated in Figure 6A. The time lags of pre-onset processing to word entropy showed a gradual

advanced trend as noise increased. The time lag was approximately from around -300 ms to -180 ms at the

no-noise level (cluster-level $p < .05$) and was from around -400 ms to -250 ms at the low-noise level

(cluster-level $p < .05$), from around -630 ms to -360 ms at the high-noise level (cluster-level $p < .01$). We

estimated the peak amplitude and peak latency for the pre-onset negative peak at each SNR level. The peak

latencies were significantly different among the three SNR levels (rmANOVA, $F(2, 36) = 58.08$, $p < .001$),

and post-hoc t-tests revealed that as noise increased the peak latencies were gradually earlier ($ps < .05$,

Bonferroni corrected), as shown in Figure 6C. No significant differences were found in the peak amplitudes

(rmANOVA, $F(2, 36) = 0.63$, $p = .538$).

The pre-onset TRF responses to word entropy exhibited different spatiotemporal patterns at three SNR

levels. At the no-noise level, the ROIs included frontal-parietal electrodes and exhibited obvious left

lateralization. At the low-noise level, the ROIs showed similar left-lateralized topological distribution but

included more electrodes, while at the high-noise level, no obvious lateralization was observed in the

frontal-parietal ROIs.

444   The reconstruction accuracies from corresponding ROIs/TOIs were significantly higher in the actual

445 decoders than in the control decoders at both the low-noise level ($p < .05$, FDR corrected) and the high-

446 noise level ($p < .001$, FDR corrected), but only marginally significant at the no-noise level ($p = .073$, FDR

447 corrected), as shown in Figure 6B. Comparing the reconstruction accuracies among different SNR levels

448 revealed no significant differences (rmANOVA, $F(2, 36) = 1.64$, $p = .208$, Figure 6C).

449 **Figure 6.** Semantic-level TRF responses to word entropy in the delta band at different SNR levels. (A) The

450 bold curves in different shades of green are the mean of TRFs averaged among ROIs across participants at

451 the three SNR levels. The grey curves are TRFs averaged among the ROIs of each participant. The colored

452 horizontal line at the bottom of each plot indicates TOIs over which TRFs differed significantly from the

453 control models. Dots in the corresponding topographies depicted the ROIs. (B) Reconstruction accuracy

calculated from the ROIs/TOIs in (A). AM means actual models. CM means control models. (C) Noise

effect on the peak amplitude, peak latency, and reconstruction accuracy. Grey dots indicate data points from

each participant. Error bars denote the standard error. n.s.: not significant, †: $p < .1$, *: $p < .05$, **: $p < .01$,

***: $p < .001$.

3.5 Correlation between TRF responses and behavioral performance

As the peak latencies of both the post-onset positive peak of acoustic-level TRFs and the pre-onset

negative peak of semantic-level TRFs showed significant differences among SNR levels, we then created

linear mixed effect models to explore whether these peak latencies were sensitive predictors of the

behavioral performance with the following general formula:

$$Behavioral\ performance \sim SNR(+Peak\ latency)(+SNR:Peak\ latency) + Random \quad (6)$$

where "Behavioral performance" refers to the comprehension performance, clarity, or intelligibility ratings.

"SNR" takes the values of speech intensity percentage, i.e., 100%, 60%, and 40%. "Peak latency" refers to

the peak latencies of either the acoustic-level post-onset TRFs or the semantic-level pre-onset TRFs,

depending on the specific model being investigated. "SNR:Peak latency" refers to the interaction between

them. A random intercept per participant was included in the model. "Peak latency" and "SNR:Peak latency"

were added between brackets to the general formula because these factors were included only if they led to

a lower Akaike Information Criterion (AIC) which indicated a better fitting (Verschueren et al., 2022).

Results showed that overall, the behavioral performance was correlated with SNR levels, which echoed the

behavioral results in the section 3.1. More importantly, the earlier peak latencies of semantic-level pre-

onset TRF response were correlated with the decreasing comprehension performance (LME, $\beta = 2.61 \times 10^{-4}$,

$t(52.64) = 1.853$, $p = .069$) and the decreasing perceived intelligibility (LME, $\beta = 9.26 \times 10^{-4}$, $t(40.48) =$

3.497, $p = .001$). And the correlation with intelligibility was more prominent as noise increased (LME

interaction, $\beta = -7.69 \times 10^{-4}$, $t(45.80) = -1.987$, $p = .053$), as illustrated in Table 1 and Figure 7. The

relationships between the reconstruction accuracies and the behavioral performance were also examined

through Spearman's correlation and summarized in Supplementary Table S5 and Table S6.

Table 1. LME models of the behavioral performance as a function of SNR and peak latency. Each row

indicates a different model. The SNR was given as a percentage (100%, 60%, 40%).

		SNR			Peak latency			SNR:Peak latency		
		β	t	p	β	t	p	β	t	p
Comprehension performance	TRF$_{acoustic}$	1.46×10^{-2}	3.835	.001	No lower AIC			No lower AIC		
	TRF$_{semantic}$	6.23×10^{-2}	1.056	.297	2.61×10^{-4}	1.853	.069	No lower AIC		
Clarity	TRF$_{acoustic}$	8.87×10^{-1}	16.481	< .001	No lower AIC			No lower AIC		
	TRF$_{semantic}$	8.87×10^{-1}	16.481	< .001	No lower AIC			No lower AIC		
Intelligibility	TRF$_{acoustic}$	1.74×10^{-1}	6.050	< .001	No lower AIC			No lower AIC		
	TRF$_{semantic}$	-1.34×10^{-1}	-1.147	.257	9.26×10^{-4}	3.497	.001	-7.69×10^{-4}	-1.987	.053

481   **Figure 7.** Correlation between the peak latencies of the semantic-level pre-onset TRFs and (A) the

482   comprehension performance and (B) the perceived intelligibility. Colored dots indicate data points from

483   each participant at different SNR levels.

4 Discussion

The current study investigated the neural tracking of hierarchical features of naturalistic speech in noisy situations using a TRF-based technique. Significant post-onset acoustic-level TRF responses were found within the central electrodes at around 400 ms, and the peak latencies were delayed as noise increased. Significant pre-onset semantic-level TRF responses were found within the frontal electrodes at around -600~-200 ms. The peak latencies showed a gradually advanced trend as noise increased, and increased advancement was correlated with decreasing comprehension performance and intelligibility. These findings indicated that noise differently modulates acoustic and semantic processing and suggested that robust and adaptive semantic pre-activation could play a vital role in reliable speech comprehension in noisy environments.

The delayed peak latency in the acoustic-level TRF responses as noise increased was in line with several previous studies, suggesting an impaired efficiency in challenging conditions with background noise (Gillis, Decruy, et al., 2022; Mirkovic et al., 2019; Muncke et al., 2022; Yasmin et al., 2023; Zou et al., 2019). As the frontally and centrally distributed channels (corresponding to the primary auditory cortex, superior temporal gyrus, premotor cortex, etc.) have been frequently reported to be related to the processing of speech acoustics (e.g., Bidelman & Howell, 2016; Broderick et al., 2019; Hickok & Poeppel, 2007; Zou et al., 2019), the present TRF results would imply similar recruitment of these brain regions for acoustic-level processing for naturalistic speech under various SNR levels. However, the post-onset 400-ms latency was later compared to the commonly reported latency of < 300 ms in previous studies (Gillis, Decruy, et al., 2022; Yasmin et al., 2023). This discrepancy could be due to the causal filter used for EEG signal preprocessing in the present study, possibly resulting in a delayed TRF compared to previous studies using noncausal filters, similar as reported by Etard and Reichenbach (2019). Alternatively, it could be possible that the latency modulation started earlier but only reached significance later for the present dataset, as the observed TRF responses exhibited an oscillatory pattern starting much earlier than 400 ms (Figure 5C). While an impaired processing efficiency has been associated with both amplitude and latency modulation by noise in previous studies (Muncke et al., 2022; Zion Golumbic et al., 2013; Zou et al., 2019), the present study together with a series of other studies reporting latency-only results would suggest latency as a more

sensitive candidate for noisy speech processing (Ding & Simon, 2013; Kaplan-Neeman et al., 2006;

Whiting et al., 1998).

At the semantic level, our findings on the pre-onset response to word entropy were consistent with

recent studies, in which the neural responses to entropy have been reported to involve neural activities

within the left hemisphere at up to 800 ms before onset (Goldstein et al., 2022; Weissbart et al., 2020;

Willems et al., 2016). This pre-onset prediction mechanism for the upcoming stimuli was regarded as a

fundamental computational principle in the human language processing (Goldstein et al., 2022). Our results

echo these findings and highlight the potential of entropy as a promising index for exploring forward-

looking prediction mechanisms.

More importantly, our results extend the present understanding of the predictive mechanism with the

manipulation of the SNR levels and suggest a distinct mechanism for speech-in-noise comprehension at the

semantic level. The significant pre-onset response to word entropy appeared at all SNR levels, which would

imply that such a forward-looking prediction was robust against noise. In addition, we found that the peak

latencies of the pre-onset responses became earlier with increasing noise, and that increased forward shift

trend at each SNR level was correlated with poorer perceived intelligibility as well as decreasing

comprehension performance. One possible explanation for this phenomenon is that our brain could adjust

the timing of predictive processing in response to adverse environments. As semantic prediction can

facilitate speech comprehension (Mattys et al., 2012; Miller et al., 1951; Obleser & Kotz, 2010; Pickering

& Gambi, 2018; Zekveld et al., 2011), the brain relies on it more heavily as noise increases to counteract

distorted auditory input. Nevertheless, noise can increase the processing load and decrease the processing

efficiency (Gillis, Decruy, et al., 2022; Kaplan-Neeman et al., 2006; Kong et al., 2014; Mirkovic et al.,

2019). To compensate for the interference, the neural system initiates the pre-onset response earlier and

extends it for a longer duration, giving our brain more time for the preparation of the upcoming speech

information. The more degraded the speech, the greater the need for this kind of "early-bird" compensation.

Another possible explanation is that in noisy environments our brain relies more on longer-range prediction

based on higher-level context information to enhance speech comprehension. According to a recent study

based on GPT-2 and functional Magnetic Resonance Imaging (fMRI) (Caucheteux et al., 2023), the

forward-looking prediction involved hierarchical representations and multiple time scales, with the

539 maximum of forecast distance reaching 8 words (corresponding to approximately 3.15s). Future studies

540 could employ local and context-unified entropy (e.g., Brodbeck et al., 2022) and longer time windows to

541 further elucidate the noise effect on the forward-looking prediction. Overall, our findings suggest that the

542 brain has a robust and adaptive prediction mechanism for reliable speech comprehension in noisy

543 environments. As such a pre-onset signature was not observed at the acoustic level, our results suggest the

544 predictive mechanism might be mainly focused at the semantic level (Goldstein et al., 2022; Grisoni et al.,

545 2021), where the speech information is expected to be more abstract and more robust against noise (Yasmin

546 et al., 2023).

547  Interestingly, the spatial patterns of TRF responses to word entropy showed left-lateralization at the

548 no-and low-noise levels and recruited bilateral hemispheres at the high-noise level. The left-lateralization

549 has been reported in studies on speech-in-noise comprehension (Z. Li et al., 2021) and was found to be

550 sensitive to linguistic content (Peelle et al., 2013), word entropy (Willems et al., 2016), and semantic

551 expectancy (Golestani et al., 2013; Obleser & Kotz, 2010). Our results would support the left-lateralized

552 brain regions for predictive speech processing at the semantic level. Meanwhile, research has reported that

553 regions within the right hemisphere, such as the right inferior frontal gyrus, are sensitive to semantic

554 features such as entropy (Willems et al., 2016) and that the involvement of the right hemisphere increased

555 under degraded conditions (Bidelman & Howell, 2016), which was hypothesized as the possible

556 recruitment of additional regions for compensation (Shtyrov et al., 1998, 1999). Accordingly, our results

557 suggest that the involvement of bilateral hemispheric in adverse environments might reflect a semantic-

558 related compensation mechanism.

559  Our results suggested the specificity of the frequency band for processing different levels of speech

560 information. Specifically, acoustic-level TRF response was primarily associated with the theta band

561 whereas semantic-level TRF neural response was dominated by the delta band (Figure 4). This could be

562 explained as that theta- and delta-band neural tracking have different functional roles: the former is related

563 to acoustic processing while the latter is related to sematic/syntactic processing (Dai et al., 2022; Ding et

564 al., 2014; Etard & Reichenbach, 2019; Kösem & van Wassenhove, 2017; J. Li et al., 2023). Alternatively,

565 this distinction could be related to the intrinsic temporal properties of the speech features (Lalor, 2018),

566 that is, a faster acoustic-level fluctuation at the theta rhythm and a slower semantic-level fluctuation at the

word rate similar to the delta rhythm. Further studies could employ careful experimental manipulation to

clarify whether this frequency-specific neural tracking is the result of intrinsic neural oscillations or

stimulus-evoked responses (see a review, Obleser & Kayser, 2019). For instance, researchers could

manipulate the speech rate (Oganian et al., 2023) and examine whether the frequency characteristics of

neural tracking at the semantic level change in response to the varying word rates.

The present study has some limitations to be noted. First, there were several significant TRF responses

to word entropy not included in the above analyses and discussions, which were primarily observed at the

no-noise level. As the focus of the present study was speech-in-noise comprehension, these responses were

not further discussed. Nevertheless, they also reflected speech information processing that would deserve

investigations in future studies. Second, while the present study only adopted word entropy and word

surprisal as two semantic-level features (Gillis et al., 2021; Goldstein et al., 2022; Heilbron et al., 2022;

Weissbart et al., 2020; Willems et al., 2016), the rapid development in NLP methods especially the large

language models (LLMs) present us with a broader range of options such as semantic embedding (Heilbron

et al., 2022). Future studies could employ additional indexes to fully demonstrate the adaptation mechanism

of speech-in-noise comprehension. Furthermore, beyond feature extraction, the LLMs also could serve as

brain-aligned agents which could be compared with humans and help unveil shared (or unique) mechanisms

in the human brain (Caucheteux et al., 2023; Goldstein et al., 2022; Mahowald et al., 2023; Schrimpf et al.,

2020). In sum, future studies could employ the promising NLP-based approach to further extend our

understanding of language processing. Third, despite the advantage of the high temporal resolution of EEG

in exploring temporal dynamics, the relatively poor spatial resolution limits the ability to investigate brain

regions involved in predictive mechanisms. A more fine-grained analysis of the spatiotemporal dynamics

of semantic prediction would require techniques such as fMRI, ECoG, or multimodal approaches.

In summary, the current study investigated how noise affected acoustic and semantic processing during

naturalistic speech comprehension. With increasing noise, acoustic processing became increasingly delayed

whereas semantic processing became increasingly advanced. Our results suggest that, while the efficiency

of brain processing of speech information is indeed impaired by noise, the brain could compensate for the

associated effects through active prediction at the semantic level. Overall, the present findings are expected

to contribute to the growing research on the neural mechanisms of naturalistic speech comprehension in

noisy environments.

Funding

This work was supported by the National Natural Science Foundation of China (NSFC) and the German Research Foundation (DFG) in project Crossmodal Learning (NSFC 62061136001/DFG TRR-169/C1, B1), and the National Natural Science Foundation of China (61977041).

Author contributions

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Declaration of competing interest

All the co-authors declare that they have no conflict of interest.

Data availability statement

Data in the current study are openly available in the Open Science Framework at https://osf.io/de9p6/, reference number DOI 10.17605/OSF.IO/DE9P6.

Acknowledgment

The authors would like to thank Prof. Xiaoqin Wang for providing the shielded room for the experiment. The authors would like to thank Prof. Zhiyuan Liu and members of his lab for computing the NLP models. The authors would like to thank Lingyi Tao and Xuelin Wang for their help with data collection.

References

Alday, P. M. (2019). M/EEG analysis of naturalistic stories: A review from speech to language processing. *Language, Cognition and Neuroscience*, *34*(4), 457–473. https://doi.org/10.1080/23273798.2018.1546882

Alexandrou, A. M., Saarinen, T., Kujala, J., & Salmelin, R. (2020). Cortical entrainment: What we can learn from studying naturalistic speech perception. *Language, Cognition and Neuroscience*, *35*(6), 681–693. https://doi.org/10.1080/23273798.2018.1518534

Aydelott, J., Dick, F., & Mills, D. L. (2006). Effects of acoustic distortion and semantic context on event-related potentials to spoken words. *Psychophysiology*, *43*(5), 454–464. https://doi.org/10.1111/j.1469-8986.2006.00448.x

Benjamini, Y., & Hochberg, Y. (1995). Controlling the False Discovery Rate: A Practical and Powerful Approach to Multiple Testing. *Journal of the Royal Statistical Society: Series B (Methodological)*, *57*(1), 289–300. https://doi.org/10.1111/j.2517-6161.1995.tb02031.x

Bidelman, G. M., & Howell, M. (2016). Functional changes in inter- and intra-hemispheric cortical processing underlying degraded speech perception. *NeuroImage*, *124*(Pt A), 581–590. https://doi.org/10.1016/j.neuroimage.2015.09.020

Billings, C. J., Bennett, K. O., Molis, M. R., & Leek, M. R. (2011). Cortical encoding of signals in noise: Effects of stimulus type and recording paradigm. *Ear and Hearing*, *32*(1), 53–60. https://doi.org/10.1097/AUD.0b013e3181ec5c46

Billings, C. J., Tremblay, K. L., Stecker, G. C., & Tolin, W. M. (2009). Human evoked cortical activity to signal-to-noise ratio and absolute signal level. *Hearing Research*, *254*(1), 15–24. https://doi.org/10.1016/j.heares.2009.04.002

Brainard, D. H. (1997). The Psychophysics Toolbox. *Spatial Vision*, *10*(4), 433–436.

Brodbeck, C., Bhattasali, S., Cruz Heredia, A. A., Resnik, P., Simon, J. Z., & Lau, E. (2022). Parallel processing in speech perception with local and global representations of linguistic context. *ELife*, *11*, e72056. https://doi.org/10.7554/eLife.72056

Brodbeck, C., & Simon, J. Z. (2020). Continuous speech processing. *Current Opinion in Physiology*, *18*, 25–31. https://doi.org/10.1016/j.cophys.2020.07.014

Broderick, M. P., Anderson, A. J., Di Liberto, G. M., Crosse, M. J., & Lalor, E. C. (2018). Electrophysiological Correlates of Semantic Dissimilarity Reflect the Comprehension of Natural, Narrative Speech. *Current Biology*, *28*(5), 803-809.e3. https://doi.org/10.1016/j.cub.2018.01.080

Broderick, M. P., Anderson, A. J., & Lalor, E. C. (2019). Semantic Context Enhances the Early Auditory Encoding of Natural Speech. *Journal of Neuroscience*, *39*(38), 7564–7575. https://doi.org/10.1523/JNEUROSCI.0584-19.2019

Broderick, M. P., Di Liberto, G. M., Anderson, A. J., Rofes, A., & Lalor, E. C. (2021). Dissociable electrophysiological measures of natural language processing reveal differences in speech

comprehension strategy in healthy ageing. *Scientific Reports*, *11*(1), 4963.

https://doi.org/10.1038/s41598-021-84597-9

Caucheteux, C., Gramfort, A., & King, J.-R. (2023). Evidence of a predictive coding hierarchy in the

human brain listening to speech. *Nature Human Behaviour*, 1–12. https://doi.org/10.1038/s41562-

022-01516-2

Connolly, J. F., Phillips, N. A., Stewart, S. H., & Brake, W. G. (1992). Event-related potential sensitivity

to acoustic and semantic properties of terminal words in sentences. *Brain and Language*, *43*(1), 1–

18. https://doi.org/10.1016/0093-934X(92)90018-A

Crosse, M. J., Di Liberto, G. M., Bednar, A., & Lalor, E. C. (2016). The Multivariate Temporal Response

Function (mTRF) Toolbox: A MATLAB Toolbox for Relating Neural Signals to Continuous

Stimuli. *Frontiers in Human Neuroscience*, *10*. https://doi.org/10.3389/fnhum.2016.00604

Crosse, M. J., Zuk, N. J., Di Liberto, G. M., Nidiffer, A. R., Molholm, S., & Lalor, E. C. (2021). Linear

Modeling of Neurophysiological Responses to Speech and Other Continuous Stimuli:

Methodological Considerations for Applied Research. *Frontiers in Neuroscience*, *15*, 1350.

https://doi.org/10.3389/fnins.2021.705621

Dai, B., McQueen, J. M., Terporten, R., Hagoort, P., & Kösem, A. (2022). Distracting Linguistic

Information Impairs Neural Tracking of Attended Speech. *Current Research in Neurobiology*,

100043. https://doi.org/10.1016/j.crneur.2022.100043

Daltrozzo, J., Wioland, N., & Kotchoubey, B. (2012). The N400 and Late Positive Complex (LPC)

Effects Reflect Controlled Rather than Automatic Mechanisms of Sentence Processing. *Brain

Sciences*, *2*(3), Article 3. https://doi.org/10.3390/brainsci2030267

de Cheveigné, A., & Nelken, I. (2019). Filters: When, Why, and How (Not) to Use Them. *Neuron*,

102(2), 280–293. https://doi.org/10.1016/j.neuron.2019.02.039

Di Liberto, G. M., O'Sullivan, J. A., & Lalor, E. C. (2015). Low-frequency cortical entrainment to speech

reflects phoneme-level processing. *Current Biology*, *25*(19), 2457–2465.

https://doi.org/10.1016/j.cub.2015.08.030

Ding, N., Chatterjee, M., & Simon, J. Z. (2014). Robust cortical entrainment to the speech envelope relies

on the spectro-temporal fine structure. *NeuroImage*, *88*, 41–46.

https://doi.org/10.1016/j.neuroimage.2013.10.054

Ding, N., & Simon, J. Z. (2013). Adaptive temporal encoding leads to a background-insensitive cortical

representation of speech. *Journal of Neuroscience*, *33*(13), 5728–5735.

https://doi.org/10.1523/JNEUROSCI.5297-12.2013

Ding, N., & Simon, J. Z. (2014). Cortical entrainment to continuous speech: Functional roles and

interpretations. *Frontiers in Human Neuroscience*, *8*, 311.

https://doi.org/10.3389/fnhum.2014.00311

Donhauser, P. W., & Baillet, S. (2020). Two distinct neural timescales for predictive speech processing.

Neuron, *105*(2), 385–393. https://doi.org/10.1016/j.neuron.2019.10.019

Etard, O., & Reichenbach, T. (2019). Neural Speech Tracking in the Theta and in the Delta Frequency
Band Differentially Encode Clarity and Comprehension of Speech in Noise. *Journal of*
Neuroscience, *39*(29), 5750–5759. https://doi.org/10.1523/JNEUROSCI.1828-18.2019
Fuglsang, S. A., Dau, T., & Hjortkjær, J. (2017). Noise-robust cortical tracking of attended speech in real-
world acoustic scenes. *NeuroImage*, *156*, 435–444.
https://doi.org/10.1016/j.neuroimage.2017.04.026
Gillis, M., Decruy, L., Vanthornhout, J., & Francart, T. (2022). Hearing loss is associated with delayed
neural responses to continuous speech. *European Journal of Neuroscience*, *55*(6), 1671–1690.
https://doi.org/10.1111/ejn.15644
Gillis, M., Van Canneyt, J., Francart, T., & Vanthornhout, J. (2022). Neural tracking as a diagnostic tool
to assess the auditory pathway. *Hearing Research*, 108607.
https://doi.org/10.1016/j.heares.2022.108607
Gillis, M., Vanthornhout, J., Simon, J. Z., Tom Francart, & Brodbeck, C. (2021). Neural markers of
speech comprehension: Measuring EEG tracking of linguistic speech representations, controlling the
speech acoustics. *Journal of Neuroscience*. https://doi.org/10.1523/JNEUROSCI.0812-21.2021
Giraud, A.-L., & Poeppel, D. (2012). Cortical oscillations and speech processing: Emerging
computational principles and operations. *Nature Neuroscience*, *15*(4), 511–517.
https://doi.org/10.1038/nn.3063
Goldstein, A., Zada, Z., Buchnik, E., Schain, M., Price, A., Aubrey, B., Nastase, S. A., Feder, A.,
Emanuel, D., Cohen, A., Jansen, A., Gazula, H., Choe, G., Rao, A., Kim, C., Casto, C., Fanda, L.,
Doyle, W., Friedman, D., … Hasson, U. (2022). Shared computational principles for language
processing in humans and deep language models. *Nature Neuroscience*, *25*(3), 369–380.
https://doi.org/10.1038/s41593-022-01026-4
Golestani, N., Hervais-Adelman, A., Obleser, J., & Scott, S. K. (2013). Semantic versus perceptual
interactions in neural processing of speech-in-noise. *NeuroImage*, *79*, 52–61.
https://doi.org/10.1016/j.neuroimage.2013.04.049
Grisoni, L., Miller, T. M., & Pulvermüller, F. (2017). Neural Correlates of Semantic Prediction and
Resolution in Sentence Processing. *Journal of Neuroscience*, *37*(18), 4848–4858.
https://doi.org/10.1523/JNEUROSCI.2800-16.2017
Grisoni, L., Tomasello, R., & Pulvermüller, F. (2021). Correlated Brain Indexes of Semantic Prediction
and Prediction Error: Brain Localization and Category Specificity. *Cerebral Cortex*, *31*(3), 1553–
1568. https://doi.org/10.1093/cercor/bhaa308
Hamilton, L. S., & Huth, A. G. (2020). The revolution will not be controlled: Natural stimuli in speech
neuroscience. *Language, Cognition and Neuroscience*, *35*(5), 573–582.
https://doi.org/10.1080/23273798.2018.1499946
Hartley, C. A., & Poeppel, D. (2020). Beyond the Stimulus: A Neurohumanities Approach to Language,
Music, and Emotion. *Neuron*, *108*(4), 597–599. https://doi.org/10.1016/j.neuron.2020.10.021

Heilbron, M., Armeni, K., Schoffelen, J.-M., Hagoort, P., & de Lange, F. P. (2022). A hierarchy of
linguistic predictions during natural language comprehension. *Proceedings of the National Academy*
of Sciences of the United States of America, *119*(32), e2201968119.
https://doi.org/10.1073/pnas.2201968119

Hickok, G., & Poeppel, D. (2007). The cortical organization of speech processing. *Nature Reviews*
Neuroscience, *8*(5), 393–402. https://doi.org/10.1038/nrn2113

IBM corp. (2019). *IBM SPSS statistics for Macintosh* (26.0) [Computer software]. IBM corp.

Jamison, C., Aiken, S. J., Kiefte, M., Newman, A. J., Bance, M., & Sculthorpe-Petley, L. (2016).
Preliminary Investigation of the Passively Evoked N400 as a Tool for Estimating Speech-in-Noise
Thresholds. *American Journal of Audiology*, *25*(4), 344–358. https://doi.org/10.1044/2016_AJA-15-
0080

Kaplan-Neeman, R., Kishon-Rabin, L., Henkin, Y., & Muchnik, C. (2006). Identification of syllables in
noise: Electrophysiological and behavioral correlates. *The Journal of the Acoustical Society of*
America, *120*(2), 926–933. https://doi.org/10.1121/1.2217567

Keitel, A., Ince, R. A., Gross, J., & Kayser, C. (2017). Auditory cortical delta-entrainment interacts with
oscillatory power in multiple fronto-parietal networks. *Neuroimage*, *147*, 32–42.
https://doi.org/10.1016/j.neuroimage.2016.11.062

Kingma, D., & Ba, J. (2015). Adam: A method for stochastic optimization. *International Conference on*
Learning Representations, ICLR. https://doi.org/10.48550/arXiv.1412.6980

Koerner, T. K., Zhang, Y., Nelson, P. B., Wang, B., & Zou, H. (2017). Neural indices of phonemic
discrimination and sentence-level speech intelligibility in quiet and noise: A P3 study. *Hearing*
Research, *350*, 58–67. https://doi.org/10.1016/j.heares.2017.04.009

Kong, Y.-Y., Mullangi, A., & Ding, N. (2014). Differential modulation of auditory responses to attended
and unattended speech in different listening conditions. *Hearing Research*, *316*, 73–81.
https://doi.org/10.1016/j.heares.2014.07.009

Kösem, A., & van Wassenhove, V. (2017). Distinct contributions of low- and high-frequency neural
oscillations to speech comprehension. *Language, Cognition and Neuroscience*, *32*(5), 536–544.
https://doi.org/10.1080/23273798.2016.1238495

Koskinen, M., Kurimo, M., Gross, J., Hyvärinen, A., & Hari, R. (2020). Brain activity reflects the
predictability of word sequences in listened continuous speech. *NeuroImage*, *219*, 116936.
https://doi.org/10.1016/j.neuroimage.2020.116936

Kutas, M., & Federmeier, K. D. (2011). Thirty Years and Counting: Finding Meaning in the N400
Component of the Event-Related Brain Potential (ERP). *Annual Review of Psychology*, *62*(1), 621–
647. https://doi.org/10.1146/annurev.psych.093008.131123

Kutas, M., & Hillyard, S. A. (1984). Brain potentials during reading reflect word expectancy and
semantic association. *Nature*, *307*(5947), 161–163. https://doi.org/10.1038/307161a0

Lakatos, P., Gross, J., & Thut, G. (2019). A New Unifying Account of the Roles of Neuronal
Entrainment. *Current Biology*, *29*(18), R890–R905. https://doi.org/10.1016/j.cub.2019.07.075

Lalor, E. C. (2018). Neuroscience: The Rhythms of Speech Understanding. *Current Biology*, *28*(3),
R105–R108. https://doi.org/10.1016/j.cub.2017.12.038

Li, J., Hong, B., Nolte, G., Engel, A. K., & Zhang, D. (2021). Preparatory delta phase response is
correlated with naturalistic speech comprehension performance. *Cognitive Neurodynamics*.
https://doi.org/10.1007/s11571-021-09711-z

Li, J., Hong, B., Nolte, G., Engel, A. K., & Zhang, D. (2023). *EEG-based speaker-listener neural
coupling reflects speech-selective attentional mechanisms beyond the speech stimulus* (p.
2022.10.02.510499). bioRxiv. https://doi.org/10.1101/2022.10.02.510499

Li, Z., Hong, B., Wang, D., Nolte, G., Engel, A. K., & Zhang, D. (2022). Speaker–listener neural
coupling reveals a right-lateralized mechanism for non-native speech-in-noise comprehension.
Cerebral Cortex, bhac302. https://doi.org/10.1093/cercor/bhac302

Li, Z., Li, J., Hong, B., Nolte, G., Engel, A. K., & Zhang, D. (2021). Speaker–Listener Neural Coupling
Reveals an Adaptive Mechanism for Speech Comprehension in a Noisy Environment. *Cerebral
Cortex*, *bhab118*. https://doi.org/10.1093/cercor/bhab118

Li, Z., & Zhang, D. (2023). How does the human brain process noisy speech in real life? Insights from the
second-person neuroscience perspective. *Cognitive Neurodynamics*. https://doi.org/10.1007/s11571-
022-09924-w

Mahowald, K., Ivanova, A. A., Blank, I. A., Kanwisher, N., Tenenbaum, J. B., & Fedorenko, E. (2023).
Dissociating language and thought in large language models: A cognitive perspective
(arXiv:2301.06627). arXiv. https://doi.org/10.48550/arXiv.2301.06627

Maris, E., & Oostenveld, R. (2007). Nonparametric statistical testing of EEG- and MEG-data. *Journal of
Neuroscience Methods*, *164*(1), 177–190. https://doi.org/10.1016/j.jneumeth.2007.03.024

Martin, B. A., & Stapells, D. R. (2005). Effects of low-pass noise masking on auditory event-related
potentials to speech. *Ear and Hearing*, *26*(2), 195–213. https://doi.org/10.1097/00003446-
200504000-00007

Mattys, S. L., Davis, M. H., Bradlow, A. R., & Scott, S. K. (2012). Speech recognition in adverse
conditions: A review. *Language and Cognitive Processes*, *27*(7–8), 953–978.
https://doi.org/10.1080/01690965.2012.705006

Mesik, J., Ray, L., & Wojtczak, M. (2021). Effects of Age on Cortical Tracking of Word-Level Features
of Continuous Competing Speech. *Frontiers in Neuroscience*, *15*.
https://doi.org/10.3389/fnins.2021.635126

Miller, G. A., Heise, G. A., & Lichten, W. (1951). The intelligibility of speech as a function of the
context of the test materials. *Journal of Experimental Psychology*, *41*(5), 329.

Mirkovic, B., Debener, S., Schmidt, J., Jaeger, M., & Neher, T. (2019). Effects of directional sound
processing and listener's motivation on EEG responses to continuous noisy speech: Do normal-

hearing and aided hearing-impaired listeners differ? *Hearing Research*, *377*, 260–270.

https://doi.org/10.1016/j.heares.2019.04.005

Muncke, J., Kuruvila, I., & Hoppe, U. (2022). Prediction of Speech Intelligibility by Means of EEG

Responses to Sentences in Noise. *Frontiers in Neuroscience*, *16*.

https://doi.org/10.3389/fnins.2022.876421

Obleser, J., & Kayser, C. (2019). Neural entrainment and attentional selection in the listening brain.

Trends in Cognitive Sciences, *23*(11), 913–926. https://doi.org/10.1016/j.tics.2019.08.004

Obleser, J., & Kotz, S. A. (2010). Expectancy Constraints in Degraded Speech Modulate the Language

Comprehension Network. *Cerebral Cortex*, *20*(3), 633–640. https://doi.org/10.1093/cercor/bhp128

Obleser, J., & Kotz, S. A. (2011). Multiple brain signatures of integration in the comprehension of

degraded speech. *NeuroImage*, *55*(2), 713–723. https://doi.org/10.1016/j.neuroimage.2010.12.020

Oganian, Y., Kojima, K., Breska, A., Cai, C., Findlay, A., Chang, E. F., & Nagarajan, S. S. (2023). Phase

Alignment of Low-Frequency Neural Activity to the Amplitude Envelope of Speech Reflects

Evoked Responses to Acoustic Edges, Not Oscillatory Entrainment. *Journal of Neuroscience*,

43(21), 3909–3921. https://doi.org/10.1523/JNEUROSCI.1663-22.2023

Oostenveld, R., Fries, P., Maris, E., & Schoffelen, J.-M. (2011). FieldTrip: Open Source Software for

Advanced Analysis of MEG, EEG, and Invasive Electrophysiological Data. *Computational*

Intelligence and Neuroscience, *2011*, 1–9. https://doi.org/10.1155/2011/156869

O'Sullivan, Power, A. J., Mesgarani, N., Rajaram, S., Foxe, J. J., Shinn-Cunningham, B. G., Slaney, M.,

Shamma, S. A., & Lalor, E. C. (2015). Attentional selection in a cocktail party environment can be

decoded from single-trial EEG. *Cerebral Cortex*, *25*(7), 1697–1706.

Peelle, J. E., Gross, J., & Davis, M. H. (2013). Phase-Locked Responses to Speech in Human Auditory

Cortex are Enhanced During Comprehension. *Cerebral Cortex*, *23*(6), 1378–1387.

https://doi.org/10.1093/cercor/bhs118

Pickering, M. J., & Gambi, C. (2018). Predicting while comprehending language: A theory and review.

Psychological Bulletin, *144*(10), 1002–1044. https://doi.org/10.1037/bul0000158

Pulvermüller, F., & Grisoni, L. (2020). Semantic Prediction in Brain and Mind. *Trends in Cognitive*

Sciences, *24*(10), 781–784. https://doi.org/10.1016/j.tics.2020.07.002

Romei, L., Wambacq, I. J. A., Besing, J., Koehnke, J., & Jerger, J. (2011). Neural indices of spoken word

processing in background multi-talker babble. *International Journal of Audiology*, *50*(5), 321–333.

https://doi.org/10.3109/14992027.2010.547875

Schrimpf, M., Blank, I., Tuckute, G., Kauf, C., Hosseini, E. A., Kanwisher, N., Tenenbaum, J., &

Fedorenko, E. (2020). The neural architecture of language: Integrative modeling converges on

predictive processing. *Proceedings of the National Academy of Sciences of the United States of*

America. https://doi.org/10.1101/2020.06.26.174482

Shtyrov, Y., Kujala, T., Ahveninen, J., Tervaniemi, M., Alku, P., Ilmoniemi, R. J., & Näätänen, R.

(1998). Background acoustic noise and the hemispheric lateralization of speech processing in the

human brain: Magnetic mismatch negativity study. *Neuroscience Letters*, *251*(2), 141–144.

https://doi.org/10.1016/S0304-3940(98)00529-1

Shtyrov, Y., Kujala, T., Ilmoniemi, R. J., & Näätänen, R. (1999). Noise affects speech-signal processing

differently in the cerebral hemispheres. *NeuroReport*, *10*(10), 2189–2192. Scopus.

https://doi.org/10.1097/00001756-199907130-00034

Sohoglu, E., Peelle, J. E., Carlyon, R. P., & Davis, M. H. (2012). Predictive Top-Down Integration of

Prior Knowledge during Speech Perception. *Journal of Neuroscience*, *32*(25), 8443–8453.

https://doi.org/10.1523/JNEUROSCI.5069-11.2012

Sonkusare, S., Breakspear, M., & Guo, C. (2019). Naturalistic Stimuli in Neuroscience: Critically

Acclaimed. *Trends in Cognitive Sciences*, *23*(8), 699–714. https://doi.org/10.1016/j.tics.2019.05.004

Strauß, A., Kotz, S. A., & Obleser, J. (2013). Narrowed Expectancies under Degraded Speech: Revisiting

the N400. *Journal of Cognitive Neuroscience*, *25*(8), 1383–1395.

https://doi.org/10.1162/jocn_a_00389

Sun, M., Chen, X., Zhang, K., Guo, Z., & Liu, Z. (2016). *THULAC: An Efficient Lexical Analyzer for*

Chinese [Computer software].

Tomé, D., Barbosa, F., Nowak, K., & Marques-Teixeira, J. (2015). The development of the N1 and N2

components in auditory oddball paradigms: A systematic review with narrative analysis and

suggested normative values. *Journal of Neural Transmission*, *122*(3), 375–391.

https://doi.org/10.1007/s00702-014-1258-3

Verschueren, E., Gillis, M., Decruy, L., Vanthornhout, J., & Francart, T. (2022). Speech Understanding

Oppositely Affects Acoustic and Linguistic Neural Tracking in a Speech Rate Manipulation

Paradigm. *Journal of Neuroscience*. https://doi.org/10.1523/JNEUROSCI.0259-22.2022

Weissbart, H., Kandylaki, K. D., & Reichenbach, T. (2020). Cortical Tracking of Surprisal during

Continuous Speech Comprehension. *Journal of Cognitive Neuroscience*, *32*(1), 155–166.

https://doi.org/10.1162/jocn_a_01467

Whiting, K. A., Martin, B. A., & Stapells, D. R. (1998). The Effects of Broadband Noise Masking on

Cortical Event-Related Potentials to Speech Sounds /ba/ and /da/. *Ear and Hearing*, *19*(3), 218–231.

https://journals.lww.com/ear-

hearing/Abstract/1998/06000/The_Effects_of_Broadband_Noise_Masking_on_Cortical.5.aspx

Willems, R. M., Frank, S. L., Nijhof, A. D., Hagoort, P., & van den Bosch, A. (2016). Prediction During

Natural Language Comprehension. *Cerebral Cortex*, *26*(6), 2506–2516.

https://doi.org/10.1093/cercor/bhv075

Willems, R. M., Nastase, S. A., & Milivojevic, B. (2020). Narratives for Neuroscience. *Trends in*

Neurosciences, *43*(5), 271–273. https://doi.org/10.1016/j.tins.2020.03.003

Wöstmann, M., Fiedler, L., & Obleser, J. (2017). Tracking the signal, cracking the code: Speech and

speech comprehension in non-invasive human electrophysiology. *Language, Cognition and*

Neuroscience, *32*(7), 855–869. https://doi.org/10.1080/23273798.2016.1262051

Yasmin, S., Irsik, V. C., Johnsrude, I. S., & Herrmann, B. (2023). *The Effects of Speech Masking on*
Neural Tracking of Acoustic and Semantic Features of Natural Speech (p. 2023.02.10.527537).
bioRxiv. https://doi.org/10.1101/2023.02.10.527537

Zekveld, A. A., Rudner, M., Johnsrude, I. S., Festen, J. M., van Beek, J. H. M., & Rönnberg, J. (2011).
The Influence of Semantically Related and Unrelated Text Cues on the Intelligibility of Sentences in
Noise. *Ear and Hearing*, *32*(6), e16. https://doi.org/10.1097/AUD.0b013e318228036a

Zendel, B. R., Tremblay, C.-D., Belleville, S., & Peretz, I. (2015). The Impact of Musicianship on the
Cortical Mechanisms Related to Separating Speech from Background Noise. *Journal of Cognitive*
Neuroscience, *27*(5), 1044–1059. https://doi.org/10.1162/jocn_a_00758

Zion Golumbic, E. M., Ding, N., Bickel, S., Lakatos, P., Schevon, C. A., McKhann, G. M., Goodman, R.
R., Emerson, R., Mehta, A. D., & Simon, J. Z. (2013). Mechanisms underlying selective neuronal
tracking of attended speech at a "cocktail party." *Neuron*, *77*(5), 980–991.
http://dx.doi.org/10.1016/j.neuron.2012.12.037

Zou, J., Feng, J., Xu, T., Jin, P., Luo, C., Zhang, J., Pan, X., Chen, F., Zheng, J., & Ding, N. (2019).
Auditory and language contributions to neural encoding of speech features in noisy environments.
NeuroImage, *192*, 66–75. https://doi.org/10.1016/j.neuroimage.2019.02.047

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5 Supplementary materials

Figure S1. Clusters in TRF responses for different speech features at different SNR levels in the (A) delta/theta and (B) alpha/beta bands. The grey histograms show the distribution of the cluster-level test statistics from 1,000 permutations. The colored lines indicate significant clusters, and the black lines indicate nonsignificant clusters. n.c.: no cluster is formed. *: $p < .05$, **: $p < .01$, ***: $p < .001$.

Figure S2. Similarity index of acoustic-level and semantic-level clusters. The similarity index was calculated as the following formula:

$$Similarity\ index = \frac{1}{2}\left(S_{TRFs} + S_{topographies}\right)$$

Where S_{TRFs} refers to the temporal similarity, which derived from the Pearson's correlation between the averaged TRFs within the ROIs, and $S_{topographies}$ refers to the spatial similarity, which derived from the cosine similarity between topographies of the peak of clusters. Black rectangles indicate the visually identified clusters with similar spatiotemporal patterns.

Figure S3. Cluster A4a and A5b of the acoustic-level TRF responses in the theta band. (A) The bold curves
in different shades of red are the mean of TRFs averaged among ROIs across participants at the low- and
high-noise levels. The grey curves are TRFs averaged among the ROIs of each participant. The colored
horizontal line at the bottom of each plot indicates TOIs over which TRFs differed significantly from the
control models. Dots in the corresponding topographies depicted the ROIs. (B) Reconstruction accuracy
calculated from the ROIs/TOIs in (A). AM means actual models. CM means control models. (C) Noise
effect on the peak amplitude, peak latency, and reconstruction accuracy. Peak latencies were significantly
longer at the high-noise level than that at the low-noise level (paired-samples *t*-test, $t(18) = 4.72$, $p < .001$).
Reconstruction accuracies were significantly lower at the high-noise level than that at the low-noise level
(paired-samples *t*-test, $t(18) = 2.54$, $p < .05$). No significant differences were found in the peak amplitudes
(paired-samples *t*-test, $t(18) = 0.60$, $p = .558$). Grey dots indicate data points from each participant. Error
bar denotes the standard error. n.s.: not significant, *: $p < .05$, **: $p < .01$, ***: $p < .001$.

Figure S4. Cluster E5 and E6 of the semantic-level TRF responses to word entropy in the delta band. (A) The bold curves in different shades of green are the mean of TRFs averaged among ROIs across participants at the no- and low-noise levels. The grey curves are TRFs averaged among the ROIs of each participant. The colored horizontal line at the bottom of each plot indicates TOIs over which TRFs differed significantly from the control models. Dots in the corresponding topographies depicted the ROIs. (B) Reconstruction accuracy calculated from the ROIs/TOIs (A), AM means actual models. CM means control models. (C) Noise effect on the peak amplitude, peak latency, and reconstruction accuracy. No significant differences were found in the peak amplitudes (paired-samples t-test, $t(18) = 0.02$, $p = .981$), peak latencies (paired-samples t-test, $t(18) = -0.21$, $p = .834$), and reconstruction accuracies (paired-samples t-test, $t(18) = 0.95$, $p = .357$). Grey dots indicate data points from each participant. Error bar denotes the standard error. n.s.: not significant, *: $p < .05$, **: $p < .01$, ***: $p < .001$.

932   **Table S1.** Details of the Natural Language Processing model used to extract semantic features.

Type	Parameter
Model type	Long-Short Term Memory (LSTM)
Embedding size	200
Hidden units per layer	200
Number of layers	2
Initial learning rate	3
Gradient clipping	0.25
Sequence length	35
Drop out	0.2
Epoch	50
Batch size	3

933   **Table S2.** Descriptive statistics of semantic features. Std. means standard deviation.

	Number of words	Word entropy			Word surprisal		
		Mean	Range	Std.	Mean	Range	Std.
Story1	213	6.56	9.31	2.17	6.12	16.98	3.22
Story2	245	6.41	9.77	2.16	5.56	17.02	3.38
Story3	247	6.53	9.77	2.24	5.49	13.37	2.96
Story4	249	6.68	10.28	2.32	6.17	15.25	3.31
Story5	240	6.90	10.27	2.24	6.05	13.68	3.23
Story6	228	6.59	10.00	2.16	6.08	15.80	3.18
Story7	281	6.52	9.96	2.41	5.84	17.05	3.04
Story8	245	6.53	9.47	2.31	5.86	13.34	3.13
Story9	254	6.48	9.88	2.39	6.35	16.62	3.27
Story10	244	6.56	9.84	2.35	5.82	17.03	3.26
Story11	231	6.41	9.60	2.24	6.53	18.55	3.81
Story12	271	6.41	10.01	2.29	6.23	17.65	3.59
Story13	317	6.57	10.22	2.30	5.91	17.74	3.49
Story14	243	6.93	10.10	2.35	6.47	16.95	3.42
Story15	305	6.24	9.45	2.17	5.66	17.37	3.1
Story16	303	6.57	9.70	2.32	6.33	17.19	3.36
Story17	344	6.53	9.46	2.09	5.98	15.66	3.06
Story18	251	6.69	9.71	2.01	6.06	14.75	3.33
Story19	266	6.35	9.58	2.14	5.67	13.77	3.04
Story20	274	6.45	9.69	2.12	5.87	14.36	3.08
Story21	248	6.27	9.54	2.36	5.34	15.96	3.11
Story22	274	6.40	10.15	2.45	5.82	17.36	3.45
Story23	272	6.32	9.75	2.29	5.57	15.25	2.93
Story24	264	6.67	9.88	2.23	6.04	16.43	3.29
Story25	271	6.53	9.53	2.16	6.02	17.32	3.14
Story26	253	6.54	9.62	2.17	6.41	15.85	3.19
Story27	261	6.44	9.41	2.03	6.17	17.82	3.15
Story28	236	6.75	10.02	2.41	6.03	13.41	3.36
Story29	282	6.65	9.89	2.04	6.27	15.88	3.09
Story30	235	6.71	9.78	2.28	6.31	18.16	3.48

934   **Table S3.** Time lags of interests (TOIs) of each cluster in the acoustic-level TRF responses.

Cluster	Time lags of interests (TOIs)
A1	383 ~ 483 ms
A2a	406 ~ 453 ms
A2b	484 ~ 539 ms
A3a	344 ~ 383 ms
A3b	414 ~ 469 ms
A4a	406 ~ 445 ms
A4b	484 ~ 531 ms
A5a	336 ~ 383 ms
A5b	414 ~ 469 ms

935 **Table S4.** Time lags of interests (TOIs) of each cluster in the semantic-level TRF responses.

Cluster	Time lags of interests (TOIs)
E1	-297 ~ -195 ms
E2	-398 ~ -250 ms
E3	-625 ~ -359 ms
E4	-8 ~ 141 ms
E5	250 ~ 406 ms
E6	273 ~ 398 ms
E7	602 ~ 961 ms
E8	563 ~ 727 ms

936   **Table S5.** Spearman's correlation between the reconstruction accuracies of each cluster in acoustic-level

937   TRF responses and the behavioral performance. Significant correlation results are bolded (uncorrected).

	Comprehension Performance	Clarity Ratings	Intelligibility Ratings
A1	$r = .11, p = .647$	$r = -.11, p = .662$	$r = .10, p = .694$
A2a	$r = .05, p = .831$	$\boldsymbol{r = -.46, p = .047}$	$r = -.04, p = .858$
A2b	$r = .25, p = .309$	$\boldsymbol{r = -.50, p = .032}$	$r = .02, p = .926$
A3a	$r = .09, p = .702$	$\boldsymbol{r = -.52, p = .025}$	$r = .05, p = .854$
A3b	$r = -.002, p = .994$	$\boldsymbol{r = -.51, p = .028}$	$r = -.06, p = .798$
A4a	$r = .08, p = .757$	$\boldsymbol{r = -.47, p = .043}$	$r = -.08, p = .734$
A4b	$r = .18, p = .465$	$r = -.42, p = .071$	$r = .004, p = .986$
A5a	$r = .03, p = .918$	$\boldsymbol{r = -.46, p = .048}$	$r = .002, p = .997$
A5b	$r = .22, p = .361$	$\boldsymbol{r = -.52, p = .026}$	$r = .15, p = .541$

938 **Table S6.** Spearman's correlation between the reconstruction accuracies of each cluster in semantic-level

939 TRF responses and the behavioral performance. Significant correlation results are bolded (uncorrected).

	Comprehension Performance	Clarity Ratings	Intelligibility Ratings
E1	$r = -.09, p = .714$	$r = -.21, p = .394$	$r = .14, p = .560$
E2	$r = .11, p = .668$	$r = .23, p = .339$	$r = -.07, p = .762$
E3	$r = -.01, p = .997$	$r = -.30, p = .206$	$r = -.31, p = .203$
E4	$r = -.02, p = .928$	$r = -.24, p = .332$	$r = .09, p = .721$
E5	$\boldsymbol{r = .51, p = .027}$	$r = .15, p = .527$	$r = .37, p = .121$
E6	$r = .13, p = .594$	$r = -.22, p = .365$	$r = -.30, p = .215$
E7	$r = .20, p = .404$	$r = .04, p = .881$	$r = .15, p = .551$
E8	$r = .20, p = .411$	$r = -.28, p = .237$	$r = -.14, p = .575$