Characteristic differences in tibial subchondral bone changes in the post-traumatic

knee osteoarthritis model

Kohei Arakawa[1], Kei Takahata[1,3], Yuna Usami[1], Takanori Kokubun [1,2]

[1]Department of Health and Social Services, Health and Social Services, Graduate School of

Saitama Prefectural University, Saitama, Japan

[2]Department of Physical Therapy, Health and Social Services, Saitama Prefectural University,

Saitama, Japan

[3] Japan Society for the Promotion of Science, Tokyo, Japan

Authors' email addresses: KA, 2391001y@spu.ac.jp; KT, 2491006o@spu.ac.jp; YU,

2591003n@spu.ac.jp ; T. Kokubun, kokubun-takanori@spu.ac.jp

Corresponding Author: Takanori Kokubun, PhD

820 Sannomiya, Koshigaya-Shi, Saitama, 343-8540. Japan

Tel : 048-973-4123

Email : kokubun-takanori@spu.ac.jp

Running title:

Subchondral bone changes in knee osteoarthritis

ABSTRACT

Objective:

Meniscus degeneration and subchondral bone changes contribute to the development and

progression of knee OA. The purpose of this study was to reveal the relationship between

medial meniscus degeneration and characteristics of subchondral bone changes in

different models

Design:

We used the anterior cruciate ligament transection (ACL-T) model, destabilization of the

medial meniscus (DMM) model, controlled abnormal tibial translation (CATT) model

and a controlled abnormal tibial rotation (CATR) model with different mechanical

stresses. We performed histological analysis and micro computed tomography analysis,

at 4 and 6 weeks. In addition, we divided the tibial subchondral bone into four

compartments and set the regions of interest

Results:

Meniscus degeneration was observed in all groups, but there was no significant difference.

The ACL-T group showed posterior displacement of the contact area, and the DMM and

CATR groups showed lateral deviation of the medial meniscus. The region-specific

subchondral bone changes in each model showed that changes in mechanical stress due

to ACL and meniscus dysfunction, as well as changes in the contact area, affect the bony

structure of the subchondral bone differently in each region.

Conclusions:

Subchondral bone changes in different models of mechanical stress were different in each

region. In particular, changes in the contact area and increased compressive stress due to

meniscus dysfunction were suggested to promote bone formation. The results of this

study indicate that changes in alignment and contact area in the PTOA model may cause

region-specific characteristics of the subchondral bone changes.

Keywords:

osteoarthritis, subchondral bone, mechanical stress

INTRODUCTION

Knee Osteoarthritis (OA) is characterized by articular cartilage degeneration, which causes joint dysfunction. Knee OA is a disease of the entire joint, affecting the articular cartilage and surrounding tissues. In particular, the subchondral bone can cushion mechanical stresses with articular cartilage and interacts with articular cartilage.[1–4] Therefore, articular cartilage and subchondral bone are considered functional units. Post-Traumatic Osteoarthritis (PTOA) is a subtype of OA primarily caused by joint injury and includes anterior cruciate ligament (ACL) tears and meniscus injuries. Since the ACL is responsible for 86% of the anterior tibial translation[5], anterior-posterior joint instability occurs in patients with ACL tears. In addition , the meniscus is responsible for stabilizing the joint and distributing compressive stresses[6], resulting in increased compressive stresses in patients with meniscus injuries. Therefore, increased mechanical stress due to ACL and meniscus dysfunction is involved in the onset and progression of PTOA[7,8].

The relationship between knee OA progression and subchondral bone changes is thought to be that early-stage knee OA accelerates subchondral bone resorption. In contrast, late-stage knee OA accelerates subchondral bone sclerosis.[9,10] In addition, it has been reported that compressive loading on the tibia promotes bone formation[11] and that the reduction of mechanical stress by hindlimb suspension promotes bone resorption.[12] Our previous study revealed different characteristics of subchondral bone changes during the early knee OA phase between models that reproduced increased or decreased mechanical stress due to the ACL and meniscus dysfunction.[13] However, the

characteristics of subchondral bone changes are not completely understood, and further

studies are needed. The understanding of early changes in the subchondral bone is

important for the maintenance of subsequent joint function.

Previous studies have shown that the properties of articular cartilage differ between

the area covered by the meniscus and the area uncovered by the meniscus. Especially the

area covered by the meniscus is fragile.[14] In addition, degeneration of the meniscus has

also been observed in animal models of knee OA,[15] and it is thought that the meniscus

dysfunction leads to increased mechanical stress on the tibial articular surface. An

implication of these cartilage properties is the possibility that the properties of the

subchondral bone are also different and may be affected by the increased mechanical

stress caused by meniscus dysfunction. In previous studies, we focused on ACL and

meniscus dysfunction that affected cartilage and bone differentiation and established

some specific models of mechanical stress. Then, we reported the possibility that different

mechanical stresses may have different effects on the subchondral bone.[13,16] Thus, we

hypothesized that subchondral bone changes would depend on increased or decreased

mechanical stress and that the mechanical properties would differ in each region of the

tibial articular surface. Therefore, the purpose of this study was to reveal the relationship

between medial meniscus degeneration and characteristics of subchondral bone changes

in different models of mechanical stress that we had established.

MATERIALS AND METHODS

Animals and Experimental Design

This study was approved by the Animal Research Committee of Saitama

Prefectural University (approval number: 2020-1). The experimental design is illustrated

in **Figure 1A**. In this study, 40 twelve-week-old ICR (Institute for Cancer Research) male

mice were procured for the study. The mice were randomized into one of five groups:

ACL- transection (ACL-T) group (ACL-T, n = 8), controlled abnormal tibial translation

(CATT) group (CATT, n = 8), destabilization of the medial meniscus (DMM) group

(DMM, n = 8), controlled abnormal tibial rotation (CATR) group (CATR, n = 8), and

sham group (Sham, n=8). All mice were housed in plastic cages under a standard 12 h

light/dark cycle. Mice were permitted unrestricted movement within the cage and had

free access to food and water.

Figure 1. Experimental design and regions of interest

(A) Experimental design. We performed histological analysis and μCT analysis at 4 and 6 weeks.

These analysis involved the Sham group, ACL-T group, CATT group, DMM group, and CATR

group   (for each group, n = 4).

(B) Subchondral bone regions of interest. We divided the tibial subchondral bone into four regions

(MA, MP, LA, and LP regions) and performed μCT analysis.

Surgical Procedures

The surgical procedures were performed with reference to our previous study.[13,16]

ACL-T surgery, the medial capsule was exposed, and scissors were used to cut the ACL.

In the ACL-T group, shear stress increases with joint instability due to ACL tear. DMM

surgery, the medial capsule was exposed, and scissors were used to cut the medial

meniscotibial ligament (MMTL). In the DMM group, shear and compressive stress

increase due to meniscus dysfunction. CATT and CATR surgery followed the same

procedure as ACL-T and DMM surgery. These models created bone tunnels in the distal

femur and proximal tibia using a 25-gauge needle and 4-0 nylon threads threaded through

them. For the position of the bone tunnels, the CATT model was created to follow the

running of the ACL. In contrast, the position of the bone tunnels in the CATR model was

created more vertically than in the CATT model. The CATT group reduces the increase

in shear stress caused by ACL rupture by suppressing joint instability. On the other hand,

the CATR group minimizes the increase in shear stress caused by joint instability, and

compressive stress increases due to meniscus dysfunction. To cancel the differences in

intervention among the groups, a bone tunnel was also created in Sham groups, and a

nylon thread was tied loosely to maintain joint instability. Details of surgical intervention

methods are presented in Supplementary Methods (Supplementary Fig.1).

Supplementary Figure 1. Surgery for the CATT and CATR model.

(A)　　　Details of surgical intervention methods. Create bone tunnels in the femur and tibia (a).

Nylon threads are threaded through the bone tunnels and tightly tied (b).

(B)　　　Schematic diagram of the CATT and CATR models. Nylon suture suppresses anterior-

posterior joint instability caused by the ACL-T model and rotational joint instability caused by the

DMM model.

Histological Analysis

Mice were sacrificed at 4 and 6 weeks after surgery. Subsequently, the knee joint

was fixed in 4% paraformaldehyde/phosphate-buffered saline for 24 h, followed by

decalcification in 10% ethylenediaminetetraacetic acid, dehydration in 70% and 100%

ethanol and xylene, and embedding in paraffin blocks. Thin sections (6 μm) were cut in

the sagittal plane using a microtome (ROM-360; Yamato Kohki Industrial Co., Ltd.,

Saitama, Japan), stained with safranin-O/fast green, and subjected to histological

evaluation to estimate the degree of medial meniscal degeneration on one slide of each

sample. All the samples were taken with a fluorescence microscope BZ-X710(Keyence,

Tokyo, Japan), and the meniscus was taken at 20x magnification.

The mouse meniscus histological grading system established by Kwok et al.[15] was

used to evaluate the degeneration in the anterior and posterior horn of the medial meniscus.

One independent observer (KT) performed meniscus scoring on a five-point scale (0-4).

Micro-computed tomography (μCT) analysis of subchondral bone

The knee joints were scanned using a μCT system (Skyscan 1272, BRUKER, MA,

USA) with the following parameters: pixel size, 6μm; voltage, 60 kV; current, 165 μA.

Subsequently, the reconstructed image was acquired using the NRecon software

(BRUKER, MA, USA). We divided the tibial subchondral bone into four compartments

and set the regions of interest (medial anterior; MA region, medial posterior; MP region,

lateral anterior; LA region, lateral posterior; LP region) (**Fig.1B**). We then designated

volumes of interest on the 40 slides of subchondral bone in each region. Then calculated

the bone volume/tissue volume fraction (BV/TV, %) for each region of interest using

CTAn software (BRUKER, MA, USA). Subsequently, we compared regions within a

model and for comparisons between models per region.

Statistical Analysis

All analyses were performed using R Studio version 1.2.5019. The normality of the

data distribution was assessed using the Shapiro-Wilk test. Subchondral bone data were

compared using a one-way analysis of variance (ANOVA), and post hoc Tukey's test was

used. Meniscus scores were compared using the Kruskal-Wallis test and post hoc Steel-

Dwass analysis. All significance thresholds were set to 5%. Parametric data are presented

as mean ± 95% confidence interval, and nonparametric data are presented as median with

interquartile ranges [IQR].

RESULTS

Histological Analysis

Medial meniscal degeneration was evaluated 4 and 6 weeks after surgery (**Fig.2**).

We presented the histological image of the meniscus in figure 2. At 4 and 6 weeks, we

observed histologic degeneration of the medial meniscus in all groups except the Sham

group. In particular, the DMM and CATR groups showed a severe decline in the anterior

horn. However, there was no significant difference in meniscus scores at 4 and 6 weeks.

Figure 2. Histological analysis of the meniscus

(A) Representative histology of the meniscus at 4 weeks and scoring results. Except for the Sham

group, there were degenerative findings in the anterior horn of the meniscus, but there was no

significant difference in the meniscus score.

(B) Representative histology of the meniscus at 6 weeks and scoring results. Although the same

degenerative findings were seen as at 4 weeks, there was no significant difference in meniscus score.

µCT analysis of subchondral bone

To elucidate the characteristics of the subchondral bone within the model, we

compared the subchondral bone changes within the model.

First, a representative image of the contact area in the sagittal and forehead planes

for each model is shown in **Figure 3**. In the sagittal plane, the contact area of the ACL-T

group was displaced posteriorly compared to the other groups. In the frontal plane, there

was no characteristic difference in the contact area, but the medial meniscus of the DMM

and CATR groups showed deviation (**Figure 3, white arrows**).

Figure 3. Reconstructed image of the knee joint

Representative reconstructed images of the sagittal and coronal planes for each group. In the sagittal

plane, the contact area of the ACL-T group was displaced posteriorly. In the coronal plane, we

observed that the deviation of the medial meniscus in the DMM and CATR groups.

Next, we showed the results of the BV/TV in **figure 4**. There was no significant

difference in the Sham group at 4 weeks and significantly reduced in the LA region

compared with the medial posterior and posterior-lateral regions at 6 weeks (LA vs. MP,

P =.010; LA vs. LP, P = .009). In the ACLT group, BV/TV was significantly increased in

the MP region compared with the MA and LA regions at 4 weeks (MP vs. MA, P =.002;

MP vs. LA, P < .001), and significantly increased in the MP region compared with the

LA region at 6 weeks (MP vs. LA, P =.036). In the CATT group, at 4 weeks, BV/TV was

significantly increased in the MP region compared with the MA and LA regions (MP vs.

MA, P =.008; MP vs. LA, P = .001) and significantly decreased in the LA region

compared with the LP region (LA vs. LP, P =.018). At 6 weeks, BV/TV was increased

significantly in the MP region compared with the MA and LA regions (MP vs. MA, P

=.045; MP vs. LA, P = .003). In the DMM group, BV/TV was significantly increased in

the MP region compared with other regions at 4 weeks (MP vs. MA, P =.009; MP vs. LA,

P < .001; MP vs. LP, P = .001). At 6 weeks, BV/TV was significantly increased in the MP

region compared with other areas and significantly decreased in the LA region compared

with the LP region (MP vs. MA, P <.001; MP vs. LA, P < .001; MP vs. LP, P < .001; LA

vs. LP, P = .005). In the CATR group, at 4 weeks, BV/TV was significantly increased in

the MP region compared with the LA and LP regions and significantly increased in the

MA region compared with the LA region (MP vs. LA, P <.001; MP vs. LP, P = .014; MA

vs. LA, P = .018). At 6 weeks, BV/TV was significantly decreased in the MP region

compared with the LA region (MP vs. LA, P =.001).

CATR groups (ACL-T vs. DMM, P = .020; CATT vs. Sham, P = .004; CATT vs. DMM,

P < .001; CATT vs. CATR, P = .017). At 6 weeks, The DMM and CATR groups were significantly higher than the Sham and ACL-T groups, and the DMM group was significantly higher than the CATT group (DMM vs. Sham, P < .001; DMM vs. ACL-T, P < .001; CATR vs. Sham, P = .047; CATR vs. ACL-T, P = .022; DMM vs. CATT, P < .001). In the MP region, at 4 weeks, the DMM group was significantly higher than the CATT group (DMM vs. Sham, P = .003). At 6 weeks, there was no significant difference. In the LA region, at 4 weeks, the CATT group was significantly lower than the Sham and DMM groups, and the CATR group was significantly lower than the Sham and DMM groups (CATT vs. Sham, P = .010; CATT vs. DMM, P = .002; CATR vs. Sham, P = .026; CATR vs. DMM, P = .006). At 6 weeks, there was no significant difference. In the LP region, at 4 weeks, there was no significant difference. At 6 weeks, the CATR group was significantly lower than the ACL-T group (CATT vs. Sham, P = .022).

DISCUSSION

The different joint instability models showed various subchondral bone changes.[13]

However, differences in the region-specific characteristics of the subchondral bone

remain unclear. In this study, we identified differences in the characteristics of meniscus

degeneration and regional subchondral bone changes in different PTOA models.

Meniscus degeneration was a trend observed in the OA model, but no significant

differences existed between models. The region-specific subchondral bone changes in

each model showed that changes in mechanical stress due to ACL and meniscus

dysfunction, as well as changes in the contact area, affect the bony structure of the

subchondral bone differently in each region (Fig. 6). Our results suggest that the changes

in subchondral bone differ depending on the increase or decrease in mechanical stress at

each region.

Figure 6. Summary of the results of this study

The PTOA model causes different contact area changes and causes region-specific characteristics of

the subchondral bone changes.

Previous studies have shown that meniscus lesions are a risk factor for OA and that

a degenerated meniscus contributes to the progression of OA.[17–20] In addition, it is clear

that meniscus degeneration contributes to cartilage degeneration, but its effect on

subchondral bone is unclear. Our histological analysis confirmed meniscus degeneration

in all models except the Sham group, but there was no significant difference in scores. In

our previous study, we observed meniscus degeneration in DMM and CATR at 8 weeks,

but not significantly different from that in the Sham group.[16] Thus, it is possible that the

results of this study did not detect differences in meniscus degeneration between models

because of the early time point. Furthermore, these results suggest that the differences in

subchondral bone changes in the present study are not due to meniscal degeneration but

increased mechanical stress due to kinematic and contact area changes associated with

ACL and meniscal dysfunction.

Previous studies have shown that articular cartilage and subchondral bone

properties vary from region to region.[14,21–23] In this study, we performed micro-CT

analysis to elucidate the differences in subchondral bone changes in the different models.

Evaluation of the contact area revealed a shift of the contact area posteriorly in the ACL-

T group, suggesting that ACL functions inhibit anterior displacement of the tibia.

Therefore, ACL transection caused the anterior displacement of the tibia, resulting in a

change in the contact area. In addition, deviation of the medial meniscus was observed in

the DMM and CATR groups. This is consistent with our previous study.[13] The meniscus

provides structural stability and dispersion of compressive stress to the knee joint.

Therefore, it is speculated that increased compressive stress and instability due to

semilunar deviation occur in the medial region of the DMM and CATR groups.

Articular cartilage has different mechanical properties depending on the region[14],

and mechanical stress induces cartilage degeneration. Therefore, subchondral bone may

also have different mechanical properties at different regions depending on their

mechanical environment. This study revealed differences in the characteristics of each

region of the subchondral bone in different models. In the Sham group, BV/TV in the LA

region was lower than in the MP and LP regions at 6 weeks. This trend was also observed

in the other models. All models used in this study created bone tunnels in the femur and

tibia. Therefore, the effect of the creation of bone tunnels may be canceled. In the ACL-

T group, BV/TV in the MP region was higher than that in the MA and LA regions at 4

weeks, and at 6 weeks, BV/TV in the MP region tended to be higher than that in the other

regions. Previous studies have shown that cartilage degeneration in the ACL-T model

occurs in the posterior-medial region of the tibia.[24] In addition, it is clear that the ACL-T

model results in an anterior tibial translation.[13,25,26] The results of this study also showed

a posterior displacement of the contact area in the ACL-T group (Fig3). Therefore, it is

suggested that the increase in mechanical stress associated with the change in contact area

after ACL transection caused the increase in BV/TV in the MP region. In the CATT group,

as in the ACL-T group, BV/TV in the MP region was higher than that in the MA and LA

regions at 4 weeks, and at 6 weeks, BV/TV in the MP region was still higher than that in

the MA and LA regions. The CATT model suppresses abnormal tibial translation of the

ACL-T model. However, previous reports have shown that the CATT model has increased

abnormal tibial translation compared to the Sham model.[13] Therefore, the subchondral

bone changes observed in the CATT group may be related to changes in mechanical stress

due to displacement of the contact surface. In the DMM group, BV/TV in the MP region

at 4 weeks was higher than that in the other regions. At 6 weeks, BV/TV tended to be

higher in the MP and MA regions. The DMM model induces OA due to meniscus

dysfunction. Previous studies have reported that increased compressive stress and joint

instability may be responsible for cartilage degeneration in the DMM model.[27–29]

Furthermore, previous studies have reported that BV/TV in the DMM model increases in

the early stages.[30] In the results of this study, deviation of the medial meniscus was

observed in the DMM group, and the subchondral bone changes in the medial region may

be caused by the increased compressive stress associated with meniscus deviation. In the

CATR group, the MA and MP regions showed higher BV/TV at 4 weeks than the LA

region, and the MP region had higher BV/TV at 4 weeks than the LP region. The CATR

model is a model that suppresses the joint instability of the DMM model. Previous studies

have confirmed lateral deviation of the medial meniscus and meniscus degeneration in

the CATR model as well as in the DMM model.[13,16] Therefore, an increase in compressive

stress is inferred in the CATR model as well as in the DMM model, which may have

caused changes in the subchondral bone in the medial region.

We have previously reported differences in subchondral bone changes between

different mechanical stress models.[13] However, the differences in the characteristics of

each region still need to be clarified. In this study, we compared the characteristics of

different regions between models. In the MA region, at 4 weeks, BV/TV in the CATT

group decreased compared with the other groups except for the ACL-T group, and at 6w

weeks, BV/TV in the DMM and CATR groups increased compared with the other groups.

The decrease in BV/TV in the CATT group is consistent with our previous reports.[13]

However, the region-by-region analysis of this study suggests that changes in the contact

areas may be responsible for the decrease in BV/TV in the MA region in the ACL-T and

CATT groups. The DMM and CATR groups are both models of meniscus dysfunction,

and previous studies have confirmed that meniscus dysfunction increases compressive

stress.[28,29] In addition, deviation of the meniscus was also observed in both models (Fig3).

Thus, it is suggested that an increase in compressive stress may increase BV/TV. These

results suggest that ACL deficiency and meniscus dysfunction, which cause PTOA, have

different effects on subchondral bone changes. In the lateral region, BV/TV in the CATT

and CATR groups in the LA region was reduced compared to the Sham group, and a

similar trend was observed in the LP region. The CATT and CATR models suppressed

joint instability. Therefore, surgical intervention to suppress joint instability may have

affected the results. Previous studies have confirmed that the CATT and CATR models

do not limit a range of motion.[13] However, the CATT and CATR models may limit a

dynamic range of motion, which needs to be examined in the future.

There are two significant limitations to this study. In this study, we analyzed at 4

and 6 weeks after surgical intervention. The reason for this was to reveal changes in the

meniscus and subchondral bone in the early stages of OA. Therefore, we have not been

able to evaluate changes over the later stages of OA. Future studies will be required to

validate additional longer time points. The effects of bone tunneling and suppression of

joint instability on knee joint motion in mice are unclear. We have confirmed that

suppression of joint instability and creation of bone tunnels do not cause limitations in

joint range of motion. However, we have not been able to evaluate them during cage

activities such as walking. Future studies should additionally examine this point and

clarify the effects of the suppression of joint instability on joint motion.

Conclusions

In conclusion, this study showed that subchondral bone changes in different models

of mechanical stress were different in each region. In particular, changes in the contact

area and increased compressive stress due to meniscus dysfunction were suggested to

promote bone formation. It has been shown that a decrease in articular cartilage thickness

is associated with alignment changes in knee OA patients.[31] The results of this study

indicate that changes in alignment and contact area in the PTOA model may cause region-

specific characteristics of the subchondral bone changes. Further studies will be required

to elucidate the relationship between articular cartilage degeneration and subchondral

bone changes caused by alignment changes, and to identify early-stage knee OA lesions

and prevent the progression of knee OA.

Author Contributions: All authors approved the final version to be published.

Study design: KA, YU, and TK

Data collection, Histological analysis: KA and KT

Subchondral bone analysis: KA and KT

Manuscript composition: KA and TK

ACKNOWLEDGEMENTS

The author(s) received no financial support for the research, authorship, and/or
publication of this article.

DECLARATION OF CONFLICTING INTERESTS

404 The authors declare that there is no conflict of interest

Ethical Approval

407 This study was approved by the Animal Research Committee of Saitama Prefectural
408 University (Approval Number: 2020-1).

Animal Welfare

411 This study followed institutional guidelines for humane animal treatment and complied
412 with relevant legislation.

REFERENCES

1. Yuan XL, Meng HY, Wang YC, Peng J, Guo QY, Wang AY, et al. Bone-

cartilage interface crosstalk in osteoarthritis: Potential pathways and future

therapeutic strategies. *Osteoarthr Cartil*. 2014;22(8):1077-1089.

doi:10.1016/j.joca.2014.05.023

2. Findlay DM, Kuliwaba JS. Bone-cartilage crosstalk: A conversation for

understanding osteoarthritis. *Bone Res*. 2016;4(July).

doi:10.1038/boneres.2016.28

3. Findlay DM, Atkins GJ. Osteoblast-chondrocyte interactions in osteoarthritis.

Curr Osteoporos Rep. 2014;12(1):127-134. doi:10.1007/s11914-014-0192-5

4. Pan J, Zhou X, Li W, Novotny JE, Doty SB, Wang L. In situ measurement of

transport between subchondral bone and articular cartilage. *J Orthop Res*.

2009;27(10):1347-1352. doi:10.1002/jor.20883

5. Butler DL, Noyes FR, Grood ES. Ligamentous restraints to anterior-posterior

drawer in the human knee. A biomechanical study. *JBJS*. 1980;62(2).

https://journals.lww.com/jbjsjournal/Fulltext/1980/62020/Ligamentous_restraints

_to_anterior_posterior.13.aspx

6. McNulty AL, Guilak F. Mechanobiology of the meniscus. *J Biomech*.

2015;48(8):1469-1478. doi:10.1016/j.jbiomech.2015.02.008

7.   Wang LJ, Zeng N, Yan ZP, Li JT, Ni GX. Post-traumatic osteoarthritis following

ACL injury. *Arthritis Res Ther*. 2020;22(1):1-8. doi:10.1186/s13075-020-02156-

5

8.   Bansal S, Floyd ER, A Kowalski M, Aikman E, Elood P, Burkey K, et al.

Meniscal repair: The current state and recent advances in augmentation. *J Orthop*

Res. 2021;39(7):1368-1382. doi:10.1002/jor.25021

9.   Fazzalari NL, Parkinson IH. Fractal properties of subchondral cancellous bone in

severe osteoarthritis of the hip. *J Bone Miner Res*. 1997;12(4):632-640.

doi:10.1359/jbmr.1997.12.4.632

10.   Intema F, Hazewinkel HAW, Gouwens D, Biilsma JWJ, Weinans H, Lafeber F,

et al. In early OA, thinning of the subchondral plate is directly related to cartilage

damage: Results from a canine ACLT-meniscectomy model. *Osteoarthr Cartil*.

2010;18(5):691-698. doi:10.1016/j.joca.2010.01.004

11.   Berman AG, Clauser CA, Wunderlin C, Hammond MA, Wallace JM. Structural

and mechanical improvements to bone are strain dependent with axial

compression of the tibia in female C57BL/6 mice. *PLoS One*. 2015;10(6):1-16.

doi:10.1371/journal.pone.0130504

12.   Nomura M, Sakitani N, Iwasawa H, Kohara Y, Takano S, Wakimoto Y, et al.

Thinning of articular cartilage after joint unloading or immobilization. An

experimental investigation of the pathogenesis in mice. *Osteoarthr Cartil*.

2017;25(5):727-736. doi:10.1016/j.joca.2016.11.013

13.   Arakawa K, Takahata K, Enomoto S, Oka Y, Ozone K, Nakagaki S, et al. The

difference in joint instability affects the onset of cartilage degeneration or

subchondral bone changes. *Osteoarthr Cartil*. 2022;30(3):451-460.

doi:10.1016/j.joca.2021.12.002

14.   Iijima H, Aoyama T, Ito A, Tajino J, Nagai M, Zhang X, et al. Immature articular

cartilage and subchondral bone covered by menisci are potentially susceptive to

mechanical load. *BMC Musculoskelet Disord*. 2014;15(1):1-12.

doi:10.1186/1471-2474-15-101

15.   Kwok J, Onuma H, Olmer M, Lotz MK, Grogan SP, D'Lima DD.

Histopathological analyses of murine menisci: Implications for joint aging and

osteoarthritis. *Osteoarthr Cartil*. 2016;24(4):709-718.

doi:10.1016/j.joca.2015.11.006

16.   Arakawa K, Takahata K, Enomoto S, Oka Y, Ozone K, Morosawa K, et al. Effect

of Suppression of Rotational Joint Instability on Cartilage and Meniscus

469  Degeneration in Mouse Osteoarthritis Model. *Cartilage*. 2022;13(1).

470  doi:10.1177/19476035211069239

471 17. Ota S, Sasaki E, Sasaki S, Chiba D, Kimura Y, Yamamoto Y, et al. Relationship

472  between abnormalities detected by magnetic resonance imaging and knee

473  symptoms in early knee osteoarthritis. *Sci Rep*. 2021;11(1):1-9.

474  doi:10.1038/s41598-021-94382-3

475 18. Sun Y, Mauerhan DR, Honeycutt PR, Kneisl JS, Norton JH, Hanley EN, et al.

476  Analysis of meniscal degeneration and meniscal gene expression. *BMC*

477  *Musculoskelet Disord*. 2010;11. doi:10.1186/1471-2474-11-19

478 19. Englund M, Guermazi A, Roemer FW, Aliabadi P, Yang M, Lewis CE, et al.

479  Meniscal tear in knees without surgery and the development of radiographic

480  osteoarthritis among middle-aged and elderly persons: The multicenter

481  osteoarthritis study. *Arthritis Rheum*. 2009;60(3):831-839. doi:10.1002/art.24383

482 20. Shrma L, Chmiel JS, Almagor O, Dorothy D, Ali G, Bathon J, et al. Significance

483  of Pre-Radiographic MRI Lesions in Persons at Higher Risk for Knee

484  Osteoarthritis. *Arthritis Rheumatol*. 2014;66(7):1811-1819.

485  doi:10.1002/art.38611.Significance

486 21. Iijima H, Aoyama T, Ito A, Tajino J, Nagai M, Zhang X, et al. Destabilization of

the medial meniscus leads to subchondral bone defects and site-speci fi c

cartilage degeneration in an experimental rat model. *Osteoarthr Cartil*.

2014;22(7):1036-1043. doi:10.1016/j.joca.2014.05.009

22.   Yeow CH, Lau ST, Lee PVS, Goh JCH. Damage and degenerative changes in

menisci-covered and exposed tibial osteochondral regions after simulated landing

impact compression - A porcine study. *J Orthop Res*. 2009;27(8):1100-1108.

doi:10.1002/jor.20861

23.   Thambyah A, Nather A, Goh J. Mechanical properties of articular cartilage

covered by the meniscus. *Osteoarthr Cartil*. 2006;14(6):580-588.

doi:10.1016/j.joca.2006.01.015

24.   Oka Y, Murata K, Kano T, Ozone K, Arakawa K, Kokubun T, et al. Impact of

Controlling Abnormal Joint Movement on the Effectiveness of Subsequent

Exercise Intervention in Mouse Models of Early Knee Osteoarthritis. *Cartilage*.

Published online 2019. doi:10.1177/1947603519885007

25.   Murata K, Kanemura N, Kokubun T, Fujino T, Morishita Y, Onitsuka K, et al.

Controlling joint instability delays the degeneration of articular cartilage in a rat

model. *Osteoarthr Cartil*. 2017;25(2):297-308. doi:10.1016/j.joca.2016.10.011

26.   Murata K, Kokubun T, Onitsuka K, Oka Y, Kano T, Morishita Y, et al.

505  Controlling joint instability after anterior cruciate ligament transection inhibits

506  transforming growth factor-beta-mediated osteophyte formation. *Osteoarthr*

507  *Cartil*. 2019;27(8):1185-1196. doi:10.1016/j.joca.2019.03.008

508 27. Adebayo OO, Ko FC, Goldring SR, Goldring MB, Wright TM, van der Meulen

509  MCH. Kinematics of meniscal- and ACL-transected mouse knees during

510  controlled tibial compressive loading captured using roentgen

511  stereophotogrammetry. *J Orthop Res*. 2017;35(2):353-360.

512  doi:10.1002/jor.23285

513 28. Arunakul M, Tochigi Y, Goetz JE, Diestelmeier BW, Heiner AD, Rudert J, et al.

514  Replication of chronic abnormal cartilage loading by medial meniscus

515  destabilization for modeling osteoarthritis in the rabbit knee in vivo. *J Orthop*

516  *Res*. 2013;31(10):1555-1560. doi:10.1002/jor.22393

517 29. Bansal S, Miller LM, Patel JM, Meadows KD, Eby MR, Saleh KS, et al.

518  Transection of the medial meniscus anterior horn results in cartilage degeneration

519  and meniscus remodeling in a large animal model. *J Orthop Res*.

520  2020;38(12):2696-2708. doi:10.1002/jor.24694

521 30. Fang H, Huang L, Welch I, Norley C, Holdsworth DW, Beier F, et al. Early

522  Changes of Articular Cartilage and Subchondral Bone in The DMM Mouse

Model of Osteoarthritis. *Sci Rep*. 2018;8(1):1-9. doi:10.1038/s41598-018-21184-

5

31.   Robbins SM, Abram F, Boily M, Pelletier JP, Martel-Pelletier J. Relationship

between alignment and cartilage thickness in patients with non-traumatic and

post-traumatic knee osteoarthritis. *Osteoarthr Cartil*. 2019;27(4):630-637.

doi:10.1016/j.joca.2019.01.002

530