Neural Geometry from Mixed Sensorimotor Selectivity for Predictive Sensorimotor Control

Running Title: Effect of Target Motion on Reach Directionality in Motor Cortex

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SUMMARY

Although recent studies suggest that activity in the motor cortex, in addition to generating motor

outputs, receives substantial information regarding sensory inputs, it is unclear how sensory

inflows affect the motor commands. Here, we recorded population neural activity in the motor

cortex via microelectrode arrays while monkeys performed flexible manual interceptions of

moving targets. During this task, which requires predictive sensorimotor control, the activity of

most neurons in the motor cortex encoding upcoming movements, was influenced by ongoing

target motion. An orbital geometry emerged in a latent neural state space at movement onset,

suggesting that target speed modulates pre-movement activity in an orthogonal manner. This

neural geometry was further evaluated with a representational model and a recurrent neural

network (RNN) with task-specific input-output mapping. We propose that sensorimotor dynamics

can be derived from neuronal mixed sensorimotor selectivity and dynamic interaction between

modulations.

INTRODUCTION

The motor cortex, a brain region generating motor commands, is widely known for its relation to

movement kinetics[1,2] and kinematics[3–5]. Moreover, it has been reported to also carry substantial

sensory information[6–13]. Activity in the motor cortex can be strongly influenced by reference

frame[14], hand trajectory[15], and stimuli for target selection[16]; there even exists evoked activity

during visual replay related to the tracking movements[17]. However, it is unclear how such sensory

input contributes to pre-movement activity in the motor cortex.

From the dynamical systems perspective, preparatory population activity develops toward a

movement-specific optimal subspace to set initial states seeding the motor generation[18–20].

However, sensory information may change the distribution of neural states during movement in

an orthogonal fashion without affecting the motor output.

To investigate the neural dynamics shaped by concurrent sensorimotor signals, we recorded

population activity in the primary motor cortex (M1) from monkeys performing a flexible manual

interception task. Unlike previous studies constraining interception at a fixed location[9,21], our task

demands predictive spatiotemporal mappings to displace a body effector to a trial-varying

location. We found that the activity of most neurons was jointly tuned to both reach direction and

target motion via directional selectivity shifts, gain modulations, offset adjustments, or their

combinations. Strikingly, such mixed sensorimotor selectivity exists throughout the entire trial, in

contrast to the gradient of sensory-to-motor tuning from cue to movement epochs in posterior

parietal cortex (PPC) that we recently reported [22,23]. Principal component analysis (PCA) of the

neural population revealed a clear orbital neural geometry in low-dimensional space at movement

onset: The neural states were distributed in reach-direction order, and formed ringlike structures

whose slopes were determined by target-motion conditions. Neuronal simulation indicates that

these characteristics of neural population dynamics could be derived from the mixed

sensorimotor selectivity of single neurons. A recurrent neural network (RNN) trained with proper

input-output mappings offers insights into the relationship between neuronal modulation and

neural geometry in a dynamical system. We propose that this sensory modulation occurs at both

single-neuron and population levels as a general element of neural computations for predictive

sensorimotor control.

Keywords: Monkey, Neural coding, Reach, Manual interception, Multi-channel recording.

RESULTS

Mixed tuning of M1 single neurons during flexible manual interception task

Three monkeys (*Macaca mulatta,* C, G, and D, male, weight 7 to 10 kg) were trained to perform a delayed manual interception task (Figure 1A), which was modified from that utilized in our recent studies [22,23]. To initiate a trial, the monkey needed to hold the center dot of a standing touch screen for 600 ms. Then, a peripheral target appeared, either stationary or rotating around the center dot at a constant angular speed. The monkey was required to wait during a random delay (400-800 ms) until the central dot went dark (GO) and then to immediately reach to the target. Once the monkey touched the screen (Touch), the target stopped and another dot showed the touching location, in red for a successful interception or in blue for a failure. The error tolerance between the target and the touch location (reach endpoint) was 3 cm. There were five target-motion conditions, consisting of clockwise (CW) conditions - 240 °/s and -120 °/s, counterclockwise (CCW) conditions 120 °/s and 240 °/s, along with 0 °/s (static) condition. We define the target-speed magnitude as TS_{mag} (0 °/s, 120 °/s, and 240 °/s) and the target-speed direction as TS_{dir} (CCW and CW). These target-motion conditions were interleaved trial by trial, and initial location of the target was random. The reach endpoints of a well-trained monkey distributed uniformly around the circle (Figure 1B, Rayleigh's test: p=0.36; data from monkey C, 772 correct trials in one session). Because the reach direction was defined as the angle of the reach endpoint, for simplicity, we divided the circular space equally into eight sectors (45° per each), and grouped trials according to the eight reach directions and five target-motion conditions.

We recorded neural data with Utah arrays from monkeys C, G, and D (implanted sites are shown in Figure 1C, and all datasets listed in Table S1) and hand trajectories from monkeys C and G (Figure S1), during the interception task. The hand trajectory was launched to the final interception position. The temporal profiles of hand velocity were unimodal bell-like curves and similar across target-motion conditions (correlation coefficients is 0.97±0.05 for monkey C and 0.99±0.02 for monkey G).

Notably, we found that neuronal directional tuning during motor execution (MO±100 ms, MO for movement onset) was modulated by target motion, according to our statistical criteria mainly in three ways: preferred direction (PD) shift, gain, and offset addition (Figure 1D and Figure S2-S4, Methods). PD-shift neurons had their PDs shifted in moving-target conditions compared to the static-target condition. As illustrated by an example neuron (Figure 1D, *PD shift*), whose PDs corresponding to CCW conditions (red and yellow) and CW conditions (blue and purple) exhibited obvious differences, TS_{dir} rather than TS_{mag} dominated this modulation. Gain-modulation neurons exhibited reach-direction tuning multiplied by target speed: while their directionality remained invariant, the neuronal responses at PD differed across target-motion conditions. This modulation

was dominated by TS_{dir} as well. The turning curves of the example neuron (Figure 1D, *Gain*) had

higher responses at PD in CW conditions (blue and purple) than in the others (green, yellow, and

red), indicating a varying tuning depth for reach direction. Neurons with addition modulation

underwent changes of offset activity induced by target speed (both TS_{dir} and TS_{mag}). As shown by

the example neuron (Figure 1D, *Addition*), this effect was almost equal for all reach directions.

The activity of these example neurons could be well explained by PD shift, gain, and additive

models (Figure 1E, *Methods*), respectively. Nevertheless, it was difficult to classify all neurons

with mixed sensorimotor selectivity into one of these three groups exclusively, because many of

them experienced a mixture of two or three of above modulations. Moreover, the proportions of

three groups were almost equal (Table 1). We found that the adjusted R^2 of a full model (0.64 ±

0.21, mean ± sd.) was larger than that of the PD shift (0.59 ± 0.23), gain (0.56 ± 0.21), and

additive (0.47 ± 0.24) models for monkey C (95 neurons), as well as for all three monkeys (rank-

sum test, $p<0.01$, Figure S5). These target-motion modulations of neuronal directionality

suggested the participation of sensory signals in shaping neural dynamics during interception

execution.

Figure 1. Flexible manual interception task and behavioral performance

A Diagram of interception task.

B Touch endpoints distribution. Left panel shows three reaching-up example trials in five target-motion conditions. The squares label the touch endpoints, and the circles and triangles are the target onset and stop location. The five target-motion conditions (-240°/s, - 120°/s, 0°/s, 120°/s, and 240°/s) are indicated in five colors (purple, blue, green, yellow, and red). Target starting location is randomly distributed. Right panel shows that the touch endpoints had uniform distribution around the circle (monkey C 772 trials, Rayleigh's test, p=0.36).

C Implanted locations of microelectrode array in the motor cortex of the three well-trained monkeys. Neural data were recorded from the cortical regions contralateral to the used hand. AS, arcuate sulcus; CS, central sulcus.

D Three example neurons with PD shift, gain modulation, and offset addition. The peri-stimulus
time histograms (PSTH) show the activity of example neurons when monkeys reached to upper
areas in five target-motion conditions.
E The directional tuning curve of three example neurons with PD shift, gain, and addition
modulation around movement onset (MO ± 100 ms, the same neurons as in Figure 1D, adjusted
R^2 of three neurons: 0.70, 0.84, and 0.60). Dots and bars denote the average and standard error
of firing rates, respectively, colored as target-motion conditions.
135
136 **Table 1 Ratio of M1 neurons modulated by target speed around movement onset**

Proportion of various modulation neurons	Gain (G)	PD shift (S)	Addition (A)	None
Monkey C N=84.9±15.9, 7 sessions	46.9±15.9%	79.0±8.9%	61.9±14.5%	6.5±6.2%
Monkey G, N=97.5±17.7, 4 sessions	29.3±4.9%	51.6±29.1%	25.9±8.3%	25.5±15.8%
Monkey D, N=44.5±7.5, 4 sessions	45.6±13.8%	74.4±8.8%	49.1±9.1%	10.8±5.4%
RNN, N=200 100 models	30.5±3.5%	26.6±3.1%	37.9±6.6%	43.9±4.6%

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138 Single neurons were classified by comparing firing rate patterns between target-speed conditions
139 (more details in **Methods**). The first column is the mean±std. of recording unit number in one
140 monkey across sessions. The other columns give the ratio of target-speed modulation unit across
141 sessions.
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Coding of sensory and motor information in neural populations
To quantify target motion information embodied in neural response in motor cortex, we performed
a series of decoding analyses on the neural data from monkey C (n=95, 772 correct trials). To
begin with, neural data were utilized to train a support vector machine (SVM) classifier for target-
motion conditions (one in five), and another for reach directions (one in eight; Methods). As
Figure 2A shows, the decoding accuracy of the target-motion condition increased quickly and
peaked at over 70% around GO, while the decoding accuracy of reach direction climbed and
reached a plateau of about 80% before MO. These results are similar to those of the other two

monkeys and the pseudo-populations (Figure S6), suggesting that mixed sensorimotor selectivity

in M1 was sustained throughout almost the entire trial.

We then performed another decoding analysis to address whether the neural coding rules were

consistent across different target-motion conditions. We trained a reach-direction decoder (one in

eight) to check if the decoder of one certain target-motion condition could be transferred to other

conditions during execution period (Figure 2B left). It turned out that the performance of the

transferred decoder deteriorated more significantly for $TS_{dir.}$ (CCW *vs.* CW, mean ± sd. of

accuracy 0.26±0.06), compared with that for TS_{mag} (120 *vs.* 240, 0.50±0.06, paired t-test, p<0.01)

and for target's state (static *vs.* motion 0.55±0.06, paired t-test, p<0.01). This result suggests that

the coding of reach direction was rather sensitive to $TS_{dir,}$ but containing similarities for static and

moving targets. As control, we also compared the neural coding rules across different reach-

direction conditions. We trained a target-speed decoder (one in five), and similarly checked the

transferred decoding accuracy (Figure 2B right). We observed that the target-speed decoder was

locked with reach direction, as the transferred decoding accuracy diminished with increasing

difference of reach direction. These results at least qualitatively imply that the reach-directional

tuning varied with target-speeds, especially $TS_{dir.}$, and this target-speed effect was non-

directional.

To explore how sensory information influences neural dynamics while preserving motor output,

we performed PCA on the normalized population activity for four important epochs. Here, we

define the "neural states" as the projection of single-trial data during a specific time bin on

principal components[24–26]. At MO, the first two principal components (PCs) of the neural states

explained the most variance ([24.8%, 13.8%]) and were most related to reach direction (the

goodness of fitting reach direction, $[R^2_{pc1}, R^2_{pc2}]$ = [0.82, 0.81], Figure 2C). In the plane spanned by

PC1 and PC2, the neural states of single trials gradually clustered by reach direction when

approaching MO (Figure 2D). Furthermore, the neural states tended to form ringlike structures

(the goodness of fitting ellipses $R^2_{Ellipse}$ = 0.67 ± 0.06, 0.81 ± 0.04, 0.93 ± 0.01, and 0.77 ± 0.05, in

the four epochs, mean ± sd. across five target-motion conditions). Taken together, these results

suggest that target motion affects M1 neural dynamics via a topologically invariant geometric

transformation.

Figure 2. Features of encoding pattern at population level

A The decoding accuracy (SVM with 10-fold cross-validation) of reach direction (black line) and target speed (blue line) by population activity (monkey C, n=95, 772 trials), is aligned to target on (TO), GO, and movement onset (MO). The dash-dotted lines are chance level of decoding reach direction (black, one in eight) and target speed (blue, one in five). The shaded area is the standard deviation of the decoding accuracy for 10 repetitions.

B The left panel shows the performance of reach-direction decoder (one in eight) transferred between different target-motion conditions. The SVM decoder was built on randomly selected 100 trials in training dataset and tested in another 100 trials from a dataset of different conditions (CCW *vs.* CW, 120 *vs.* 240, static *vs.* motion). The distributions of decoding accuracy were from

1000 repetitions and compared with one tailed t-test (p<0.01, with three stars). The right panel

shows the performance of target-speed decoder (one in five) in different reach-direction

conditions. In this case, reach direction is grouped by eight equal sectors (each 45°), and for

each condition 60 trials were randomly selected for training and testing. The accuracy distribution

was also obtained from 1000 repetitions.

C The principal components explained variance and representation. The first row shows the

explained variance of each PC (cumulatively over 70%). The second row shows the PCs' fitting

goodness (R^2_{PCs}) of reach direction and target speed in four epochs.

D The neural state across epochs. In this plane spanned by the first two PCs, the dots represent

the single-trial neural states in color corresponding to target-speed or reach-direction. The

explained variance is marked on the corresponding axes. All state dots are colored in eight reach

directions (first row) and five target-motion conditions (second row). The goodness of fitting

ellipses ($R^2_{Ellipse}$) for the state dots under single target-motion conditions is shown by mean ± sd.

We also checked the trial-averaged neural trajectories for 40 conditions (5 target speeds x 8

reach directions) during movement preparation and execution (Figure S7). The results reflected

target-speed effects as well: First, the distance between neural trajectories grouped by reach-

direction conditions was larger than that between neural trajectories grouped by target-speed

conditions (Figure S7A, B), suggesting that M1 primarily encoded reach direction rather than

target speed, especially after GO. Second, the distance between neural trajectories of CCW and

CW was much larger than that between neural trajectories of 120°/s and 240 °/s conditions,

indicating that TS_{dir} dominated the target-speed effect (Figure S7C).

Orbital neural geometry in latent space

Next, we concentrated on the newfound neural geometry in low-dimensional space at MO. For

better visualization, we performed an affine transformation on all resulting neural state points to

make the ellipse of the static condition orthogonal to the z-axis (Figure 3A and Figure S8). As

shown in Figure 2D, the projections of the single-trial neural state onto the PC1-PC2 subspace

clustered, or rather distributed, in reach-direction order (Figure 3A top and Figure 3B left).

Interestingly, the interlocked ringlike structures in two-dimensional space disengaged from each

other in three-dimensional space, and the ellipses fitted from neural states under single target-

motion conditions exhibited concentric shapes (the fitting goodness of ellipses, $R^2 = 0.92 ± 0.01$,

mean ± sd., see Methods). Moreover, these ellipses tilted in condition-dependent angles, which is

particularly evident in the PC2-PC3 subspace (Figure 3A bottom and Figure 3B right). We

quantified the spatial features of these ellipses by calculating the tilting angles, which were

between the normal vectors of the moving-target and static-target conditions. Strikingly, this tilting

angle was linearly correlated with target speed (both TS_{mag} and TS_{dir}), and the relationship was

robust in nine datasets from three monkeys (Figure 3C and Figure S9).

Given these results, we propose that this orbital neural geometry epitomizes the sensorimotor

dynamics of M1 at the population level. The sensory input can regularly modulate neural states in

an orthogonal dimension (PC3), without interfering with motor generation (in PC1 and PC2).

Figure 3. The orbital neural geometry in latent dynamics

A Three-dimensional neural state of M1 activity obtained from PCA. As in Figure 3c, each point

represents a single trial. The upper subplot is colored according to five target speeds, while the

bottom is in colors corresponding to eight reach directions. The explained variances of the first

three PCs were 17.7%, 11.3%, and 5.9%. Neural data were collected with target-speed

modulated units (monkey C, N=480, merged six sessions) and random 15 trials in 40 conditions

(K=600 trials).

B Fitted ellipses of neural states. The ellipses fitted in [A] are projected onto three two-

dimensional spaces, colored in target speeds (left column) or reach directions (right column).

C The relative angle of ellipses. The angle is calculated between ellipses of the target-motion

condition and static-target condition (0 °/s) in the range from -90° to 90°, CCW is positive. Circles,

squares, and triangles correspond to monkeys C (7 sessions), G (4 sessions) and D (4 sessions),

respectively. The lines represent the linear relationship of ellipses angle (θ) and target speed

(sp.), with function solid line θ = 0.23*sp.+4.2, R^2=0.91 for monkey C; dashed line θ =

0.26*sp.+4.3, R^2=0.81 for monkey D; dotted line θ = 0.15*sp.-1.4, R^2=0.89 for monkey G.

Population neural geometry relies on neuronal tuning

Population neural geometry relies on neuronal tuning

We then asked whether a group of single neurons with a certain type of mixed sensorimotor

selectivity could exhibit the orbit neural geometry.

For this purpose, three neuronal models were constructed for the three typical modulations

described above (PD shift, gain, and addition, see Figure 1D and Figure S2-S4). We ran a

simulation with these representational neuronal models (Figure 4A). Here, each group consisted

of 300 model neurons with their PDs uniformly distributed, and was solely modulated as PD-shift,

gain, or addition (Methods). The resulting neural geometry of the three simulation groups showed

distinct features (Figure 4B): The single-condition ellipses were inclined with target-motion-

dependent angles in the PD-shift and gain groups, similar to the real neural data, but the ellipses

in the addition group were layered in parallel. The reach-direction clusters in the first two PCs

were conservative in the gain and addition group, but not in the PD-shift group. These results

indicate that the neural states of the real data mainly exhibit the geometry feature of the gain

modulation group. Nonetheless, we found that a population with a uniform mixture of all three

modulations was able to simulate the neural geometry as well (Figure 4C).

Comparing with the static-target condition, we calculated relative rotation angle and tilting angle

between ellipses along with the vertical shift of neural states, in order to quantify the simulated

structure (Figure 4D). The results show that the real data yielded a smaller rotation angle than the

PD-shift group, a smaller vertical shift than the additive group, but larger tilting angles than all

models. The mixed group had the most similar tilting angle, though with moderate performance in

rotation angle and state shift.

These simulations suggest that the existence of PD-shift and additive modulation would not

disrupt the neural geometry that is primarily driven by gain modulation; rather it is possible that

these three modulations support each other in a mixed population.

Figure 4. The shape of neural dynamics relies on neuronal mixed selectivity

A The tuning curves of three ideal neurons in five target-motion conditions. From up to down,
they are PD shift, gain modulation, and (offset) addition. The activity of these ideal neurons is
simulated by the multiplication of temporal Gaussian function (bin=50 ms) and the reach-direction
cosine function, also scaled by a sigmoid function involving target speed in three different ways.

B The simulated neural states from three groups, colored by target-motion conditions (first row)
and reach directions (second row). For each simulation, the neural states were obtained from 300
model neurons by PCA. The neural state in 180° reach direction is highlighted with a red marker.
The first two principal components can explain more than 95% of the variance in the data (the
explained variance of the first three PCs, Gain: 49.5%, 46.6%, and 2.0%; PD shift: 50.1%, 47.1%,
and 1.6%; Addition:50.8%, 47.9%, and 1.4%)

C The neural states of a mixed group of 100*3 model neurons, as in **B.** The explained variance of
the first three principal components were 48.4%, 44.2%, and 3.1%.

D Quantification of the difference between neural-state ellipses in four simulated groups and a
real dataset (monkey C, n=95). Rotation angle is the relative rotation angle differences in the first

two neural state. Tilting angle is the relative angle of the normal vector of ellipses. State shift is

the root mean square of the distance between two ellipses.

Recurrent neural network provides dynamic insights

To infer how such modulated subpopulations would interact with each other in a dynamical

system, we trained 100 RNN models with random weight initialization (Figure 5A; see Methods).

The inputs included motor intention, target location, and a Go signal. Motor intention was defined

as an abstract motor command predicted to compensate for sensorimotor delays[27], and could be

provided by the PPC[28,29], here simplified as the interception location. The network was to

generate hand velocity after MO. For a fixed validation set of 500 trials, these trained network

models performed well (mean square error of the reach endpoint and the target was 0.0046 ±

0.0027, a. u., mean ± sd., while the radius of target motion was 0.15).

In these network models, we found comparable features of nodes. First, most activated nodes

(for example, Figure 5B) could be classified into the above-mentioned three modulations (Table

1) by the same statistical standard as for the real neural data. Second, the states reduced from

node population activity were arranged in a way resembling the actual neural geometry at MO

(the fitting goodness of ellipses, R^2 = 0.98 ± 0.05, mean ± sd.; Figure 5C). The tilting angles

followed the same pattern as suggested by the actual results (Figure 5D).

With these RNN models, we perturbed the connection between different modulation groups.

The connections within and between gain modulation and additive modulation were stronger than

the others (Figure 5E), however, further strengthening the connection from gain to additive nodes

or within additive nodes would disorder the orbital structure more significantly (Figure S10A and

Table S2). We speculate that the influence, and perhaps the formation, of modulations both relate

to the robust input and output weight pattern across models (Figure S10B, C). These results

support strong and similar roles of gain and additive nodes, but what is even more important is

that the three modulations interact each other, so the PD-shift nodes should not be neglected.

Figure 5. The neural geometry in RNNs

A Network architecture. The network input consists of motor intention, target location, and GO signal. The motor intention is the two-dimensional Cartesian coordinates of the interception location, and exists fixed during MO-50ms to MO; the target location is the two-dimensional Cartesian coordinates of the moving target, and appears time-varying during the whole trial; the GO-signal is a step function from 0 to 1 after GO. The RNN with 200 hidden units is expected to output hand velocity as two-dimensional Cartesian coordinates for accurate interception.

B Three example nodes with PD-shift modulation, gain modulation, and addition modulation. Similar to Figure 1D.

C Three-dimensional neural state of node activity obtained from PCA, colored in target-motion conditions (top) and in reach-direction conditions (Bottom). Similar to Figure 3A.

D The relative angle of ellipses. Similar to Figure 3D. The fitted line is $\theta = 0.15 * sp. + 0.11$, $R^2 = 0.96$ for five target speeds.

334   **E** The connectivity between different types of modulations. On the left is a boxplot representing

335   the averaged absolute connection weight, across 100 models. S for PD-shift nodes, G for gain

336   nodes, and A for addition nodes. On the right is a diagram of the connectivity, with linewidth

337   representing the connection strength.

DISCUSSION

To reveal how sensory inflows influence neural dynamics during movement, we recorded M1 population activity from monkeys performing a flexible manual interception that is highly dependent on predictive sensorimotor transformations. Single-neuron activity showed that the movement tuning of M1 neurons varied with target-motion conditions in complicated ways, including PD shift, gain modulation, addition, or their mixtures. Unsupervised dimensionality reduction (PCA) on population activity revealed an orbital neural geometry, where neural states of single trials spontaneously formed ellipses and were tilted according to target-motion conditions. Such a geometry, which could be simulated with a group of representational neurons for gain modulation alone, also emerged in the RNN with appropriate input-output mappings. As suggested by a dynamic and connected population as the RNN, the interactions between modulations were sophisticated in preserving the encoding of motor output. These results reveal sensory modulation of pre-movement neural dynamics at the single-neuron and population levels, and bridge the neuronal mixed sensorimotor selectivity and a low-dimensional neural geometry, compactly representing the sensorimotor co-function.

Previous studies have showed that M1 activity is seldom evoked by purely visual stimuli, with only weak tuning[8,30,31], and has transient responses to behaviorally relevant visual cues[7,10,32–34]. In this study, the modulated neural dynamics, though distinguished according to target-motion conditions, is ultimately shaped for motor generation rather than sensory representation. It is a pity that we did not record sufficient muscle data during interception to rule out the representation of the motor cortex for kinetic variables such as force[1,26,35] , but we believe that this would not invalidate our main conclusions.

Previous studies have revealed interactions between motor kinematic variables such as reach direction and hand velocity[15,36,37]. Although the effect of arm-dependent speed (hand velocity) on reach-direction tuning may exist, it cannot fully explain neural activity during interception. First, we found hand velocity to vary with TS_{mag}, but the largest gap in neuronal activity was related to TS_{dir}. Second, for a new dataset with trials resampled to ensure similar distributions of hand velocities in five target-motion conditions, the orbital neural geometry remained similar and the target-motion gain model provided a better explanation compared to the hand-velocity gain model (Figure S11).

In the present study, we focused on the orbital neural geometry by taking 'snapshots' of neural activities with PCA. In addition to unsupervised PCA, we tried supervised dimensionality reduction methods like dPCA[38]. However, the dPCA results (Figure S12) showed that the condition-independent temporal component explained the largest variance, followed by the component of reach direction, whereas the interactive and target-speed components only covered very small proportions. The dPCA did not distinguish a target-speed dimension, probably

because reach directions were continually distributed around a circle and target speed was

primarily mixed with reach directionality.

Our simulations with neuronal models and RNN demonstrate that differences in modulations

and the interaction between them can be essential. In fact, modulations in the form of PD shift

and gain have been widely found in the motor cortex and PPC regions contributing to

sensorimotor transformation. For example, motor cortex neurons experience gain and PD shift

modulation by arm posture[35,39,40]. Neurons in PPC have eye and hand gain fields for a visually-

guided reach plan[41–43], integrating target position related to gaze and hand position to form motor

intention[28,44,45]. Therefore, we conclude that three types of modulations should all be involved in

sensorimotor computation in predictive motor control. In addition, recent studies show that

interactions of PPC-motor cortex circuity are involved in motor planning, spatial transformation

and motor selection[46–48]. The PPC-M1 circuit, as a key part of cortico-subcortical networks for the

predictive sensorimotor control[49], is a topic for future studies.

 # STAR Methods

392 **Key resources table**

REAGENT or RESOURCE	SOURCE	IDENTIFIER
Experimental models: Organisms/strains		
Rhesus macaques (Macaca mulatta)	Beijing Institute of Xieerxin Biology Resource, China	N/A
Software and algorithms		
Matlab	MathWorks	http://mathworks.com/
Python		
Other		
Cerebus System	Blackrock Microsystems	https://blackrockneurotech.com/products/cerebus/
Utah Microelectrode Arrays	Blackrock Microsystems	https://blackrockneurotech.com/products/utah-array/

Resource availability

Lead contact

Further information and requests for resources and reagents should be directed to and will be

fulfilled by the Lead Contact, Dr. He Cui (**hecui@cibr.ac.cn**).

Materials availability

This study did not generate new unique reagents

Data and code availability

The example datasets and code have been deposited in Mendeley Preview, and will be made
public as soon as the article is officially published.
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EXPERIMENTAL MODEL AND STUDY PARTICIPANT DETAILS

Monkey

Three adult male rhesus macaques (monkey C, D, and G, *Macaca mulatta*, 7-10 kg) were used in

this study. The monkeys sat in a primate chair to perform the task. The stimuli were back

projected onto a vertical touch screen (Elo Touch system; sampling at 100 Hz, spatial resolution

<0.1 mm) about 30 cm in front of the monkeys. Hand trajectory was tracked by an optical camera

(VICON Inc.) with an infrared marker on the fingertip. All animal maintenance and procedures

were in accordance with NIH guidelines and approved by the Institutional Animal Care and Use

Committee (IACUC) of Institute of Neuroscience, CAS.

METHOD DETAILS

Task and behavior

The monkeys were trained to perform a flexible manual interception task in a dark room. The task paradigm was modified based on the visually-guided reaching interception task in a previous study [22]. At the beginning, the monkey held the green center dot of a touch screen for 600 ms to initiate a trial (Figure 1A). Then, a green target dot appeared at a random location, moving in a circular path centered on the center dot. The center dot turned dark as a GO cue after a random delay (400-800 ms); then the monkey could intercept the target at any moment within 150-800 ms after the GO cue. Once any peripheral location was touched, the target stopped. The tolerance range of the touch endpoint for correct trials was within 3 cm of the target. The monkey would be rewarded with juice after each correct trial. Targets moving clockwise (CW; -240 °/s, -120 °/s) and counterclockwise (CCW; 120 °/s, 240 °/s), as well as a stationary target (0°/s), were pseudo-randomly interleaved trial by trial. Additional target speeds (-360 °/s, -180 °/s, 180 °/s, 360 °/s added) were introduced in subsequent sessions (Table S1).

Data collection

After the monkeys were adequately trained for the task (successful rate > 90%), head-posts were implanted stereotaxically under anesthesia (induced by 10 mg/kg ketamine, then sustained by 2% Isoflurane). After few weeks of recovery and adaptation, the monkeys were implanted with Utah microelectrode arrays (Blackrock Microsystems, Salt Lake City, UT) in the motor cortex of the hemisphere contralateral to the handedness (Figure 1C, 128-channel array for monkey C, 96-channel array for monkey G and D). The location of recording areas were identified by Magnetic Resonance Imaging (MRI) and cortical sulcus features. Neuronal activity was recorded via a Blackrock Microsystem 256-channel recording system, sampled at 30 kHz. We collected 85 ± 16, 45 ± 8, 98 ± 18 well-isolated units from monkey C, G, and D across sessions (mean ± sd. more details in Table S1), respectively.

Peri-stimulus time histograms (PSTHs)

The PSTHs and spike rasters of single neurons are shown in Figure 1D and Figure S2-S4. All trials were classified into forty conditions, eight reach-endpoint sectors by five target-motion conditions. Condition-averaged firing rates were calculated with 50-ms bins and smoothed with a Gaussian kernel (standard deviation = 20 ms). The standard error of firing rates was estimated from the 10 bootstrap samples in the trials of corresponding condition.

QUANTIFICATION AND STATISTICAL ANALYSIS

Classification of neuronal tuning properties

To classify target-motion modulation for single neuron reach-direction tuning, we used the

direction-averaged firing rate around movement onset (MO ± 100ms) to calculate three indexes

for each target-motion conditions: the preferred direction (PD), the tuning depth, and the offset

activity, and classified PD shift, gain, and addition groups in Table 1. The PD of each neuron for

different target-motion conditions was calculated by the weighted sum of averaged neuronal firing

rates in eight reach-direction sectors. The tuning depth of each neuron was determined by the

range (max - min) of firing rates in corresponding target-motion conditions. The offset activity of

each neuron was calculated by the mean firing rate (MO ± 100 ms) of all target-motion conditions.

Based on the PD, tuning depth and offset activity of single neurons, a neuron was classified as

'PD shift', if its PDs were significantly different between interception and static-target condition

(Watson-Williams test in circular data, CircStat by[50]); a neuron was classified as 'gain' if its tuning

depths were significantly different between interception and static-target condition (two-tailed

Wilcoxon signed-rank test, p<0.05); a neuron was classified as 'offset' if its offset activities were

significantly different between interception and static-target condition (two-tailed Wilcoxon signed-

rank test, p<0.05).

Population decoding

The population activity of the motor cortex was used to decode target motion and reach direction

by support vector machine (SVM). Neuronal firing rate was soft-normalized as

$$FR_{norm.} = \frac{FR_{raw}}{FR_{max} - FR_{min} + 5}$$

where raw firing rates was divided by the range of firing rates plus five [18]. We trained two SVM

classifiers (MATLAB function 'fitcecoc', 10-fold cross-validation) to decode reach direction (one in

eight) and target motion (one in five) of single trials in 100-ms window sliding with 50-ms step

(Figure 2A). The temporal decoding was repeated ten times to obtain the mean and standard

deviation of decoding accuracy.

We tested the generalization of reach-direction and target-motion decoders (SVM, MATLAB

function 'fitcecoc') in different conditions during execution period (MO ± 100 ms, Figure 2B). The

decoder predicted single-trial reach direction (45°, 1/8 chance level) or target motion (1/5 chance

level) across conditions based on normalized population activity. The reach-direction decoder

(Figure 2B left), which was trained by trials in a set of target-motion conditions, was tested with

trials from other target-motion conditions (CCW vs. CW, or 120 vs. 240, or static vs. motion,

randomly selected without replacement 100 trials from corresponding training-test datasets), and

the training-test decoding was repeated 1000 times to compare the distribution of accuracy with

paired t-test. The target-speed decoder (Figure 2B right), which was trained by trials in a given

reach-direction condition within 45°, was tested with trials from other reach-direction conditions.

Neural state

The population activity was stored in NKT datasets, where N, K, and T denote the number of neurons, trials, and time bins, respectively. We averaged T dimension of neural activity in a 100-ms bin (e.g., the two 50-ms bins around MO), and normalized neuronal dimension by Z-score (MATLAB function 'zscore') to get a K*N dataset. After preprocessing, we used PCA to reduce the dimension from K*N to K*C (C is the number of principal components, first two and first three PCs), and fitted the PCs with reach direction ($PC = a_1 * cos(\theta) + a_2 * sin(\theta) + c$) and target speed ($PC = \frac{a_1}{1+e^{-a_2(sp.)}} + c$) in Figure 2. Neural states of single trials were colored for target speed or reach direction and fitting ellipses with first two PCs (Figure 2D) and first three PCs (Figure 3 and Figure S5) by MATLAB package 'MatGeom'[51]. To show the relative position of ellipses in the best viewing angle, we used an isometric affine transformation to globally map all datapoints on new axes while preserving the proportional relation of distances between points. After this linear transformation, the azimuth and elevation of ellipses changed slightly, but the tilting angle between ellipses remained constant (Figure 3 and Figure S5). The tilting angles, rotation angles, and state shift were calculated between ellipses of target-motion conditions and static-target condition in each session, defining CW as negative angles and CCW as positive angles. A set of tilting angles were obtained from corresponding conditions in one dataset, and the linear regression model was used to fit all ellipses angles (θ) and target speeds (sp.) in nine sessions.

Fitting and simulating single-neuron activity

We used PD shift, gain, offset, and full models to fit neuronal activity, basing on a cosine tuning model[3]. Neurons are fitted by single-trial data. We introduced a special sigmoid function to fit the nonlinear target-speed effects because target-speed direction (CCW vs. CW) has a stronger effect than target-speed magnitude (120 vs. 240)[52,53]. The gain and additive models refer to hand-velocity gain studies[36,37,54].

In the gain model, the target-speed effects on the amplitude of cosine tuning are denoted as:

$$FR = \left(\frac{a_1}{1 + e^{-a_2(sp.)}} + c_2 \right) * cos\left(\theta - \theta_{pd}\right) + c_1$$

where FR is the firing rate at movement onset (MO ± 100 ms). θ and *sp.* are the reach direction and target speeds, respectively; θ_{pd} is the fitted preferred direction of the neuron; a_1, a_2, c_1 are constants to be fitted.

In the additive model, the target speed adjusts the offset activity, as:

$$FR = a_1 * cos\left(\theta - \theta_{pd}\right) + \frac{a_3}{1 + e^{-a_2(sp.)}} + c_1$$

with similar symbols to the gain models, plus the new constant a_3.

In the PD shift model, the target-speed effects on PDs are represented as:

517
$$FR = a_1 * cos\left(\theta - \theta_{pd} + \frac{a_3}{1 + e^{-a_2(sp.)}}\right) + c_1$$

518   with the similar symbols to the above model.

519   The full model integrates all the three of the above effects:

520
$$FR = a_1 * cos(\theta - pd_{sp}) + \frac{a_2}{1 + e^{-a_2(\mathbf{sp}.)}} + \frac{a_3}{1 + e^{-a_2(\mathbf{sp}.)}} * cos(\theta - pd_{sp}) + a_4$$

521
$$* cos\left(\theta - pd_{sp} - \frac{a_5}{1 + e^{-a_2(\mathbf{sp}.)}}\right) + c_1$$

with constants a_1, a_2, a_3, a_4, a_5.

We fitted neuronal activity with these four models (MATLAB 'fit' function), and compared the

fitting goodness with adjusted R-squares ($R^2_{adj.} = \frac{(1-r^2)(n-1)}{n-p-1}$, where n is the trial number, and p

is the degree of the polynomial).

Simulations with model neurons were based on three models to investigate the relationship

between neuronal tuning (Figure 4A) and population neural geometry (Figure 4B). We first built

three model neuron groups (each n=300) and performed PCA to get the neural state. Then, we

repeated this in a mixed group, with 100 each of PD shift, gain and additive model neurons

(Figure 4C). Model neurons had three components: cosine-tuning for reach direction ($\theta_{pd,n}$, PD

uniform distribution around circle for each neuron n), Gaussian temporal profiles (t=1:200, σ=30,

peak time $t_{\mu,n} \in N(100, 10)$, the 100-th bin is MO, random distribution for $t_{\mu,n}$ of neurons), and

distinct target-motion modulation for each group. We designed five target speed values ($sp. =$

[1,2,3,4,5]) and 64 reach directions ($\theta = 360 * \frac{[1:64]}{64}$), for 320 trials in total[55].

The gain-model neuron has a nonlinear function with target-speed effects on the amplitude:

536
$$FR_{t,n,sp.,\theta} = e^{\frac{-(t-t_{\mu,n})^2}{2*30^2}} * \left(\frac{1}{1 + e^{-g_n(sp.-3)}} * cos(\theta - \theta_{pd,n}) + 1\right)$$

537   where g_n is a random target-motion gain within [0:1] for different neurons, and modulates target-

538   motion gain in a sigmoidal function.

539   The PD-shift model neuron has target-speed change in PD:

540
$$FR_{t,n,sp.,\theta} = e^{\frac{-(t-t_{\mu,n})^2}{2*30^2}} * \left(cos\left(\theta - \theta_{pd,n} - \frac{90}{1 + e^{-s_n(sp.-3)}}\right) + 1\right)$$

541   where s_n is a random value within [0:1.5] for different neurons, and contributes to a sigmoidal

542   function with target-motion shift on neuronal PD ($\theta_{pd,n}$).

543   The additive model neuron has target-speed effects in offset:

544
$$FR_{t,n,sp.,\theta} = e^{\frac{-(t-t_{\mu,n})^2}{2*30^2}} * \left(cos(\theta - \theta_{pd,n}) + \frac{1}{1 + e^{-g_n(sp.-3)}} + 1\right)$$

where g_n is also a random value within [0:1] for different neurons, and adjusts the offset activity in

a sigmoidal function with target-motion.

The firing rates of three groups model neuron (K*N*T, 320*300*200) were averaged at MO

(mean T = [50:150]) to get the K*N (320*200) dataset for PCA. As with the real neural data, we

selected the first three PCs (K*C, 320*3) to derive the simulated neural state shown in Figure 4.

RNN training

For the inputs of RNN, motor intention appeared from MO-50 ms to MO, and was represented as

constant variables in the form of two-dimensional Cartesian coordinates; target location was

designed as time varying two-dimensional Cartesian coordinates of the target throughout the

entire trial; the Go-signal was a step function jumping from 0 to 1 at GO. The RNN consisted of

200 hidden units, and output hand velocity for accurate interception after MO.

The RNN nodes evolved according to a standard dynamic differential equation:

$$\tau\dot{x} = -x + Jr + Bu$$

where τ is a time constant (here 50 ms), x is the activity, r is the firing rates, and u means the

combined inputs. The connection matrix J of hidden layer is initiated as random in a normal

distribution (mean = 0, sigma = $g/\sqrt{N}$, g = 1.5, N = 200), and the matrix B denotes the connection

between inputs and hidden units, initiated as zero matrix. The output z is obtained by

$$z = Wr$$

where W is the read-out weight, and is expected to reproduce the desired hand velocity

generated by bell-shaped physical equation[56]. W was also initiated as zero matrix. During

training, the loss function was:

$$E = e + \alpha r_1$$

where e is the mean squared error of z and training target. r_1 is regularity [57], denoting the

magnitude of the nodes' activity and is calculated as activity squared summed across time. For

constants, $\alpha = 1e - 7$. The optimization was realized with optim.Adam() based on PyTorch, the

learning rate was 0.001.

The classification of nodes' modulation type was finished with the same procedure for real data

as above. When perturbating the connection between certain types of modulations, the selected

connection was multiplied with 1.5. This perturbation was retained for the entire trial. The

perturbed network was tested with the same test set of 500 trials as for the intact network.

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AUTHOR CONTRIBUTIONS

Y. Zhang and H. Cui designed the experiment, Y. Zhang and T. Wang collected the data, Y.
Zhang and Y. Chen analyzed the data, Y. Chen built RNNs, Y. Zhang performed the simulation,
Y. Zhang, Y. Chen, T Wang, and H. Cui prepared the manuscript.

DECLARATION OF INTERESTS

The authors declare no conflict of interests.

REFERENCES

1. Evarts, E. V. Relation of pyramidal tract activity to force exerted during voluntary movement. *J. Neurophysiol.* **31**, 14–27 (1968).

2. Tanaka, H. Modeling the motor cortex: Optimality, recurrent neural networks, and spatial dynamics. *Neurosci. Res.* **104**, 64–71 (2016).

3. Georgopoulos, A., Kalaska, J., Caminiti, R. & Massey, J. On the relations between the direction of two-dimensional arm movements and cell discharge in primate motor cortex. *J. Neurosci.* **2**, 1527–1537 (1982).

4. Omrani, M., Kaufman, M. T., Hatsopoulos, N. G. & Cheney, P. D. Perspectives on classical controversies about the motor cortex. *J. Neurophysiol.* **118**, 1828–1848 (2017).

5. Wang, T., Chen, Y. & Cui, H. From Parametric Representation to Dynamical System: Shifting Views of the Motor Cortex in Motor Control. *Neurosci. Bull.* (2022) doi:10.1007/s12264-022-00832-x.

6. Rizzolatti, G., Scandolara, C., Matelli, M. & Gentilucci, M. Afferent properties of periarcuate neurons in macaque monkeys. II. Visual responses. *Behav. Brain Res.* **2**, 147–163 (1981).

7. Lamarre, Y., Busby, L. & Spidalieri, G. Fast ballistic arm movements triggered by visual, auditory, and somesthetic stimuli in the monkey. I. Activity of precentral cortical neurons. *J. Neurophysiol.* **50**, 1343–1358 (1983).

8. Merchant, H., Battaglia-Mayer, A. & Georgopoulos, A. P. Effects of Optic Flow in Motor Cortex and Area 7a. *J. Neurophysiol.* **86**, 1937–1954 (2001).

9. Merchant, H., Battaglia-Mayer, A. & Georgopoulos, A. P. Neural responses in motor cortex and area 7a to real and apparent motion. *Exp. Brain Res.* **154**, 291–307 (2004).

10. Rao, N. G. & Donoghue, J. P. Cue to action processing in motor cortex populations. *J. Neurophysiol.* **111**, 441–453 (2014).

11. Hatsopoulos, N. G. & Suminski, A. J. Sensing with the Motor Cortex. *Neuron* **72**, 477–487 (2011).

12. Sobinov, A. R. & Bensmaia, S. J. The neural mechanisms of manual dexterity. *Nat. Rev. Neurosci.* **22**, 741–757 (2021).

13. Suway, S. B. & Schwartz, A. B. Activity in Primary Motor Cortex Related to Visual Feedback. *Cell Rep.* **29**, 3872-3884.e4 (2019).

14. Pesaran, B., Nelson, M. J. & Andersen, R. A. Dorsal Premotor Neurons Encode the Relative Position of the Hand, Eye, and Goal during Reach Planning. *Neuron* **51**, 125–134 (2006).

15. Paninski, L., Fellows, M. R., Hatsopoulos, N. G. & Donoghue, J. P. Spatiotemporal Tuning
of Motor Cortical Neurons for Hand Position and Velocity. *J. Neurophysiol.* **91**, 515–532
(2004).

16. Cisek, P. & Kalaska, J. F. Neural Correlates of Reaching Decisions in Dorsal Premotor
Cortex: Specification of Multiple Direction Choices and Final Selection of Action. *Neuron*
45, 801–814 (2005).

17. Tkach, D., Reimer, J. & Hatsopoulos, N. G. Congruent Activity during Action and Action
Observation in Motor Cortex. *J. Neurosci.* **27**, 13241–13250 (2007).

18. Churchland, M. M. *et al.* Neural population dynamics during reaching. (2012)
doi:10.1038/nature11129.

19. Shenoy, K. V, Sahani, M. & Churchland, M. M. Cortical Control of Arm Movements: A
Dynamical Systems Perspective. *Annu. Rev. Neurosci.* **36**, 337–359 (2013).

20. Vyas, S., Golub, M. D., Sussillo, D. & Shenoy, K. V. Computation Through Neural
Population Dynamics. *Annu. Rev. Neurosci.* **43**, 249–275 (2020).

21. Merchant, H., Battaglia-Mayer, A. & Georgopoulos, A. P. Neural Responses during
Interception of Real and Apparent Circularly Moving Stimuli in Motor Cortex and Area 7a.
Cereb. Cortex **14**, 314–331 (2004).

22. Li, Y., Wang, Y. & Cui, H. Eye-hand coordination during flexible manual interception of an
abruptly appearing, moving target. *J. Neurophysiol.* **119**, 221–234 (2018).

23. Li, Y., Wang, Y. & Cui, H. Posterior parietal cortex predicts upcoming movement in
dynamic sensorimotor control. *Proc. Natl. Acad. Sci.* **119**, e2118903119 (2022).

24. Mante, V., Sussillo, D., Shenoy, K. V. & Newsome, W. T. Context-dependent computation
by recurrent dynamics in prefrontal cortex. *Nature* **503**, 78–84 (2013).

25. Parthasarathy, A. *et al.* Mixed selectivity morphs population codes in prefrontal cortex.
Nat. Neurosci. **20**, 1770–1779 (2017).

26. Sun, X. *et al.* Cortical preparatory activity indexes learned motor memories. *Nature* **602**,
274–279 (2022).

27. Cui, H. Forward Prediction in the Posterior Parietal Cortex and Dynamic Brain-Machine
Interface. *Front. Integr. Neurosci.* **10**, 1–6 (2016).

28. Andersen, R. A. & Buneo, C. A. Intentional maps in posterior parietal cortex. *Annu Rev*
Neurosci **25**, 189–220 (2002).

29. Andersen, R. A. & Cui, H. Intention, Action Planning, and Decision Making in Parietal-
Frontal Circuits. *Neuron* **63**, 568–583 (2009).

30. Kwan, H. C., Mackay, W. A., Murphy, J. T. & Wong, Y. C. Properties of visual cue
responses in primate precentral cortex. *Brain Res.* **343**, 24–35 (1985).

31.   Kruse, W. Temporal Relation of Population Activity in Visual Areas MT/MST and in
Primary Motor Cortex during Visually Guided Tracking Movements. *Cereb. Cortex* **12**,
466–476 (2002).

32.   Alexander, G. E. & Crutcher, M. D. Neural representations of the target (goal) of visually
guided arm movements in three motor areas of the monkey. *J. Neurophysiol.* **64**, 164–178
(1990).

33.   Lurito, J. T., Georgakopoulos, T. & Georgopoulos, A. P. Cognitive spatial-motor
processes. 7. The making of movements at an angle from a stimulus direction: studies of
motor cortical activity at the single cell and population levels. *Exp. Brain Res.* **87**, 562–580
(1991).

34.   Port, N. L., Kruse, W., Lee, D. & Georgopoulos, A. P. Motor Cortical Activity during
Interception of Moving Targets. *J. Cogn. Neurosci.* **13**, 306–318 (2001).

35.   Scott, S. H. & Kalaska, J. F. Reaching Movements With Similar Hand Paths But Different
Arm Orientations. I. Activity of Individual Cells in Motor Cortex. *J. Neurophysiol.* **77**, 826–
852 (1997).

36.   Moran, D. W. & Schwartz, A. B. Motor Cortical Representation of Speed and Direction
During Reaching. *J. Neurophysiol.* **82**, 2676–2692 (1999).

37.   Inoue, Y., Mao, H., Suway, S. B., Orellana, J. & Schwartz, A. B. Decoding arm speed
during reaching. *Nat. Commun.* **9**, 1–14 (2018).

38.   Kobak, D. *et al.* Demixed principal component analysis of neural population data. *Elife* **5**,
1–36 (2016).

39.   Kakei, S., Hoffman, D. S. & Strick, P. L. Muscle and Movement Representations in the
Primary Motor Cortex. *Science (80-.).* **285**, 2136–2139 (1999).

40.   Kakei, S., Hoffman, D. S. & Strick, P. L. Direction of action is represented in the ventral
premotor cortex. *Nat. Neurosci.* **4**, 1020–1025 (2001).

41.   Batista, A. P., Buneo, C. a, Snyder, L. H. & Andersen, R. a. Reach Plans in Eye-Centered
Coordinates. *Science (80-.).* **285**, 257–260 (1999).

42.   Buneo, C. a, Jarvis, M. R., Batista, A. P. & Andersen, R. a. Direct visuomotor
transformations for reaching. *Nature* **416**, 632–636 (2002).

43.   Chang, S. W. C., Papadimitriou, C. & Snyder, L. H. Using a Compound Gain Field to
Compute a Reach Plan. *Neuron* **64**, 744–755 (2009).

44.   Andersen, R. A., Snyder, L., Bradley, D. & Xing, J. Multimodal Representation of Space in
the Posterior Parietal Cortex and Its Use in Planning Movements. *Annu. Rev. Neurosci.*
20, 303–330 (1997).

45.   Cohen, Y. E. & Andersen, R. A. A common reference frame for movement plans in the
posterior parietal cortex. *Nat. Rev. Neurosci.* **3**, 553–562 (2002).

46.   Schaffelhofer, S. & Scherberger, H. Object vision to hand action in macaque parietal,
premotor, and motor cortices. *Elife* **5**, 1–24 (2016).
47.   Dann, B., Michaels, J. A., Schaffelhofer, S. & Scherberger, H. Uniting functional network
topology and oscillations in the fronto-parietal single unit network of behaving primates.
Elife **5**, 1–27 (2016).
48.   Martínez-Vázquez, P. & Gail, A. Directed interaction between monkey premotor and
posterior parietal cortex during motor-goal retrieval from working memory. *Cereb. Cortex*
28, 1866–1881 (2018).
49.   Brozović, M., Gail, A. & Andersen, R. A. Gain mechanisms for contextually guided
visuomotor transformations. *J. Neurosci.* **27**, 10588–10596 (2007).
50.   Berens, P. CircStat : A MATLAB Toolbox for Circular Statistics. *J. Stat. Softw.* **31**, 128–
129 (2009).
51.   Legland, D. MatGeom library for geometric computing with MATLAB.
52.   Pouget, A. & Sejnowski, T. J. Spatial transformations in the parietal cortex using basis
functions. *J. Cogn. Neurosci.* **9**, 222–37 (1997).
53.   Churchland, M. M. & Lisberger, S. G. Shifts in the population response in the middle
temporal visual area parallel perceptual and motor illusions produced by apparent motion.
J. Neurosci. **21**, 9387–9402 (2001).
54.   Amirikian, B. & Georgopulos, A. P. Directional tuning profiles of motor cortical cells.
Neurosci. Res. **36**, 73–79 (2000).
55.   Michaels, J. A., Dann, B. & Scherberger, H. Neural Population Dynamics during Reaching
Are Better Explained by a Dynamical System than Representational Tuning. *PLoS*
Comput. Biol. **12**, 1–22 (2016).
56.   Kao, T. C., Sadabadi, M. S. & Hennequin, G. Optimal anticipatory control as a theory of
motor preparation: A thalamo-cortical circuit model. *Neuron* **109**, 1567-1581.e12 (2021).
57.   Sussillo, D., Churchland, M. M., Kaufman, M. T. & Shenoy, K. V. A neural network that
finds a naturalistic solution for the production of muscle activity. *Nat. Neurosci.* **18**, 1025–
1033 (2015).
727
728