Ventral dentate gyrus-dominated LFP rhythmicity in the social brain reflects the context of social encounters

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Abstract

Mammalian social behavior is highly context-sensitive. Yet, nothing is known about the mechanisms that

modulate social behavior according to its context. Recent studies have revealed a network of mostly limbic

brain regions, here termed the "social brain", which regulates social behavior. We hypothesized that

coherent theta and gamma rhythms couple regions of the social brain into functional networks in a

context-dependent manner. To test this concept, we simultaneously recorded extracellular activity from

multiple social brain regions in mice performing three social discrimination tasks. Local field potential

rhythmicity during a task was mainly sensitive to an internal arousal state. However, during stimulus

investigation we observed a distinct state, which was sensitive to stimulus characteristics. Yet, the

coherence between the various regions was most sensitive to the social context. Moreover, we found the

ventral dentate gyrus to play a pivotal role in coordinating the context-specific rhythmic activity in the

network.

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17 <u>Brain-region name abbreviations</u>
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AcbC: Accumbens nucleus, core
AcbSh: Accumbens nucleus, shell
AhiAL: Amygdalo-hippocampal area, anterolateral part
BLA: Basolateral amygdaloid nucleus
BMP: Basomedial amygdaloid nucleus, posterior part
DMD: Dorsomedial hypothalamic nucleus, dorsal part
EA: Extended amygdala
IL: Infralimbic prefrontal cortex
LS: Lateral septum
MeAD: Medial amygdaloid nucleus, anterodorsal
Pir: Piriform cortex
PLH: Peduncular part of the lateral hypothalamus
PrL: Prelimbic prefrontal cortex
PVN: Paraventricular hypothalamic nucleus
vCA1: Field CA1 of the hippocampus, ventral part
vDG: Dentate gyrus, ventral part
VP: Ventral pallidum

Introduction

Mammalian social behavior is highly complex and dynamic, involving multiple types of distinct, sometimes even opposing, interactions between partners. Indeed, the identity of a partner can completely change the nature and trajectory of social actions taken by an individual (Adolphs, 2010). In addition to these complexities, social interactions are highly dependent upon the social context. For example, humans will most likely respond differently to a hand placed upon their shoulder from behind if this happens in a frightening context, such as in a dark alley in a foreign city, than if the same contact occurs in a cocktail party. Presently, little is known of the brain mechanisms and neural circuits that encode the context of social encounters and change responses to social cues accordingly.

In the last two decades, studies have begun to reveal the brain circuits that sub-serve various types of social behavior (for recent review papers see for example Ford and Young, 2021; Kohl and Dulac, 2018; McKinsey et al., 2018; Wei et al., 2021). Such studies exposed the involvement of a vast network of mostly sub-cortical limbic brain regions, here termed the "social brain" (Insel and Fernald, 2004), in processing social sensory cues and regulating mammalian social behavior (Dickinson et al., 2022; Goodson, 2005). These include striatal regions, such as the nucleus accumbens core (AcbC) and shell (AcbSh), the prelimbic (PrL) and infralimbic (IL) prefrontal cortical areas, several hippocampal and septal areas and multiple amygdaloid and hypothalamic nuclei (Dai et al., 2022; Felix-Ortiz and Tye, 2014; Kingsbury et al., 2020; Leroy et al., 2018). Many of these areas are highly interconnected in a bidirectional manner (Kohl et al., 2018; Scheggia et al., 2022; Swanson et al., 2020; Twining et al., 2017; Yamamoto et al., 2018), and some were shown to be involved in various, at times opposing, types of social behavior (Dai et al., 2022; Dolen et al., 2013; Felix-Ortiz et al., 2016; Huang et al., 2020; Reis et al., 2021). It remains, however, unclear how this intricate network of brain areas generates the large repertoire of distinct types of social behavior. Recent studies using multi-site brain recordings from behaving animals have demonstrated that system-level neural activity in sub-networks of the social brain predict individual social preferences (Mague et al., 2022) and decision-making (Schaich Borg et al., 2017) better than does local neural activity at any single brain region. These results thus suggest that coding of the various aspects of social behavior in the brain should be considered at the system level.

Oscillatory neural activity, mostly in the theta (4-12 Hz) and gamma (30-80 Hz) bands, was reported in many cortical and sub-cortical brain regions in various species (Buzsaki and Draguhn, 2004; Harris and Gordon, 2015a; Uhlhaas et al., 2009), with its power being shown to intensify during demanding cognitive functions, such as learning (Bocchio et al., 2017; Chen et al., 2021; Taub et al., 2018) and social communication (John et al., 2022; Kuga et al., 2022; Tendler and Wagner, 2015). Furthermore, abnormal

theta and gamma rhythms have been reported in multiple neurodevelopmental disorders (Buzsaki and
Watson, 2012; Cannon et al., 2014; Uhlhaas et al., 2010), such as autism spectrum disorder (ASD)
(Geschwind and Levitt, 2007; Lazaro et al., 2019). Accordingly, one prominent hypothesis states that
coherent manifestation of these rhythms can dynamically coordinate the activity of neural ensembles
dispersed over multiple brain regions and link them into *ad hoc* functional networks (Fries, 2015).
In the present study, we hypothesized that coherent theta and gamma rhythms couple various regions of
the social brain into functional networks in a social context-dependent manner. In other words, distinct
social contexts dictate different patterns of coordinated rhythmic activity of dispersed social brain
neuronal ensembles, which in turn subserve context-dependent processing of social cues and consequent
behavioral responses. To test this hypothesis, we recorded extracellular electrical activity simultaneously
from multiple regions of the social brain in mice performing three distinct binary social discrimination
tasks (contexts). The same type of social stimulus served as either preferred or less-preferred stimulus in
all three tasks. Using this design, we could link distinct patterns of rhythmic neural activity across the
social brain to either stimulus identity or its valence, or to the social context. Our results reveal that the
pattern of coordinated oscillatory activity (coherence) in the network is strongly correlated with the social
context and carries information that may be used to discriminate between distinct, albeit similar, social
contexts. Further, we revealed that the ventral dentate gyrus (vDG), an area previously linked to
contextual information (Chen et al., 2020; McHugh et al., 2007), seems to play a pivotal role in
coordinating the coherent activity among the various regions of the social brain.

Results

Analyzing the behavior of CD1 male mice during three distinct binary social discrimination tasks

Using custom-built electrode arrays (EAr; Fig. S1A) we simultaneously acquired local field potential (LFP) signals from up to 16 brain regions at a time (cumulative count: 18 regions; Figure S1B and Table S1) during interactions of adult male mice (subjects) with various stimuli (Mohapatra et al., 2022). Specifically, we employed three distinct binary social discrimination tasks (Jabarin et al., 2021; Netser et al., 2020), namely the social preference (SP), (Fig 1A), emotional-state preference (EsP) (Fig. 1E) and sex preference (SxP) (Fig 1I) tasks (Jabarin et al., 2021). Each task comprised a five min-long baseline period involving empty chambers located at opposite corners of the arena, followed by a five min-long encounter period, when a distinct stimulus was introduced into each chamber (Netser et al., 2019). Mice performing the SP task tended to interact with social stimuli (conspecifics) for significantly more time than with objects throughout the encounter period (Fig. 1B-D). Similarly, mice performing the EsP task preferred to interact with socially isolated rather than group-housed stimuli (Fig. 1E-H), while mice performing the SxP task tended to interact more with female than with male stimuli (Fig 1I-L). Thus, in each task, the subjects discriminated between a preferred and a less-preferred stimulus. Notably, the same type of stimulus (a male group-housed mouse) that was the preferred stimulus in the SP task was the less-preferred stimulus in the other two tasks. Therefore, these set of tasks allowed us to analyze brain-wide neural activity patterns in association with either the type of stimulus (i.e., a group-housed male vs. an object/group-housed female/isolated male) or its valence (i.e., preferred vs. less-preferred), or the social context (i.e., the SP, EsP or SxP task).

We further compared multiple behavioral parameters across the various tasks. There were no significant differences between the tasks in terms of total time dedicated to stimulus investigation (Fig. 1M), the total number of transitions made by the subjects between the two stimuli (Fig. 1N) or the distance traveled by the subjects during a task (Fig. 1O). Nonetheless, the preference (reflected by the relative discrimination index, RDI) between the two stimuli was lower in the EsP task, as compared to the SP task (Fig. 1P). Overall, subject behavior was similar across the various tasks.

Figure 1. Similar behavior of subject mice across three binary social discrimination tasks.

A. A track of subject movements during an SP task session, super-imposed onto a picture of the arena. The two stimuli types are indicated above their chambers.

B. Heat maps of investigation bouts made by the subjects toward each of the stimuli (stimulus type is noted above) across the five min-long encounter period of the SP task, with color-coding of the investigation bout duration (see scale on the right of the panel). Each line represents a distinct session.

C. Mean (±SEM) time dedicated by a subject for investigating each stimulus during the SP task sessions shown in B. Wilcoxon matched pairs signed rank test, n = 33 sessions, W = -495, ****p<0.0001.

D. As in C, plotted vs. time using one min bins.

E-H. As in A-D, for the EsP task. Paired t-test, n = 28 sessions, t (27) =2.374, *p = 0.025.

I-L.   As in A-D, for the SxP task. Paired t-test, n = 26 sessions, t (25) =5.75, ****p<0.0001.

M. Mean (±SEM) total time dedicated by a subject to investigate both stimuli during the encounter stage

of a task.

N. Mean (±SEM) number of transitions between stimuli made by the subject during the encounter period

of each task.

O. Mean (±SEM) distance traveled by the subjects during the encounter stage of each task.

P. Mean (±SEM) RDI for each task. Kruskal-Wallis test, n = 3 tests, 87 sessions, H = 8.509, p = 0.0142;

Dunn's *post-hoc* test, *p<0.05.

Different tasks elicit different profiles of rhythmic LFP signals in multiple brain regions

The power spectral density (PSD) profiles of LFP signals recorded during the encounter period (Fig. 2A-B),

differed among the various tasks performed by the same subject in a brain region-specific manner (Fig

S1C). For quantitative comparison, we calculated the change in power (relative to baseline) during each

task for each brain region in both the theta ($\Delta\theta$P, 4-12 Hz) and gamma ($\Delta\gamma$P, 30-80 Hz) bands. In almost

all cases, we found that the mean power of both rhythms was enhanced during the encounter period, as

compared to baseline. Notably, the mean power change differed significantly among the various tasks

and specific brain regions (Fig. 2C-D). The similar patterns of $\Delta\theta$P and $\Delta\gamma$P across the various regions

suggested the existence of a link between them. Accordingly, we found statistically significant correlation

(Pearson's, r>0.25, p<0.05) between $\Delta\theta$P and $\Delta\gamma$P for the SP and SxP tasks, while borderline significant

correlation (r=0.45, p=0.059) was observed for the EsP task (Fig. 2E-G). Thus, when measured over the

course of the entire session, both rhythms seem to be driven by the same process. When averaged across

all brain regions, both $\Delta\theta$P and $\Delta\gamma$P were highest for the SP task, compared to the other two (Fig 2H-I).

Thus, despite the generally similar behavior exhibited by subjects across the tasks (Fig. 1), their system-

level brain LFP signals significantly and consistently differed in power across tasks. Specifically, despite

involving only one social stimulus, the SP task induced the strongest LFP rhythmicity.

Figure 2. Brain region- and context-specific changes in the levels of theta and gamma power during a

social encounter.

A.   Color-coded spectrogram of LFP signals recorded in the AcbSh during the baseline (left) and

encounter (right) periods of SP task. The black line at 300 s represent the time of stimuli introduction

into the arena. The color-coding scale is shown on the right.

B.   PSD profiles of the baseline (blue) and encounter (red) periods shown in A. The gray areas mark the

theta and gamma ranges. The inset shows the theta range in higher resolution.

C.   Mean (±SEM) change in theta power (ΔθP) during the encounter period, relative to the baseline

period for each brain region in the three contexts (2-way ANOVA. Contexts: $F_{(2, 659)} = 3.838$, $p =$

0.0220; Brain regions: $F_{(17, 659)} = 1.727$, $p = 0.0341$; Interaction: $F_{(34, 659)} = 0.4548$, $p = 0.9970$)

D.   As in C, for gamma power (ΔγP; 2-way ANOVA. Contexts: $F_{(2, 659)} = 1.459$, $P = 0.2333$; Brain regions:

$F_{(17, 659)} = 2.050$, $P = 0.0076$; Interaction: $F_{(34, 659)} = 0.5732$, $P = 0.9764$).

E.   Mean ΔγP as a function of mean ΔθP during the SP task, for each brain region. Pearson's correlation

coefficient (r) and significance (*p*) are given.

F.   As in E, for the EsP task.

G.   As in E, for the SxP task.

H.   Mean (±SEM) ΔθP, averaged across all brain regions, for each task. Welch's ANOVA, W (DFn, DFd) =

14.67 (2, 31.80), $p < 0.0001$. Dunnett's T3 multiple comparisons test, SP vs. EsP, $p = 0.0018$; SP vs. SxP,

$p = 0.0002$; EsP vs. SxP, $P = 0.2653$.

I.   As in H, for ΔγP. W (DFn, DFd) = 5.134 (2, 33.65), $p = 0.0113$. SP vs. EsP, $p = 0.0531$; SP vs. SxP, $p =$

0.0127; EsP vs. SxP, $p = 0.7467$.

J.   Super-imposed traces of ΔθP averaged across brain regions for the SP (blue), EsP (green) and SxP (red)

tasks. Time 0 min represents the time of stimuli insertion.

K.   As in J, for ΔγP.

#$p = 0.053$, *$p<0.05$, **$p<0.01$, ***$p<0.001$. See also Figs. S1, S2.

To examine the temporal dynamics of LFP rhythmicity during the various tasks, we plotted ΔθP and ΔγP

as a function of time for each task and brain region. In accordance with our previous study in rats (Tendler

and Wagner, 2015), we found that both ΔθP and ΔγP began to rise several seconds before stimulus

introduction, peaked within 20 s from this point and gradually declined in all brain regions and tasks (Fig.

S2). Thus, the dynamics of LFP rhythmicity across the session were similar among the various tasks and

did not seem to reflect the behavioral dynamics (shown in Fig. 1D, H, L). We also found no significant

correlation (Pearson's, *p*>0.05) between the mean power change and speed of the subject during any task

for either ΔθP or ΔγP (Fig. S3A-F).

Overall, these results suggest that theta and gamma rhythmicity during the encounter period are driven

by an internal brain state of arousal that shows similar temporal dynamics across tasks, independent of

the behavioral dynamics.

LFP power changes during stimulus investigation are differentially modulated across brain regions and

tasks

Despite the uniform dynamics of LFP rhythmicity in the social brain during the encounter period, it may

be differentially modulated during specific behavioral events, such as stimulus investigation. We thus

examined the possibility that during investigation bouts, ΔθP and ΔγP (henceforth termed $^\Delta$θP and $^\Delta$γP)

differ between the various stimuli and tasks. As exemplified by signals recorded from the amygdalo-

hippocampal area (AhiAl) shown in Fig. 3A-F, a Z-score analysis revealed elevation in theta power during

investigation bouts towards social but not the object stimuli in the SP task, during investigation of both

stimulus types in the EsP task and during investigation of female but not male stimuli in the SxP task. Very

similar results were obtained for gamma power (Fig. S4A-F). This analysis thus suggests a bias towards

specific stimuli in a task-specific manner. Interestingly, even though the same type of stimulus (a group-

housed male) was used in all tasks, this stimulus elicited a clear elevation in LFP rhythmicity only during

the SP and EsP tasks but not during the SxP task. These results suggest that at least for the AhiAl, the

change in LFP rhythmicity was not dictated by either the stimulus type nor by its valence.

To explore the bias in LFP rhythmicity in each task, we calculated the difference in $^\Delta$θP and $^\Delta$γP between

the two stimuli separately for each brain region. Since a possible bias of LFP rhythmicity in a given brain

region may be associated with a behavioral bias towards a specific stimulus, we examined the correlation

between the two variables. To this end, we correlated the $^\Delta$θP bias (preferred – less-preferred) to the RDI

values of each task. We found a negative correlation in a specific set of brain regions (i.e, extended (EA)

and medial (MeAD) amygdala, lateral septum (LS), paraventricular hypothalamic nucleus (PVN),

infralimbic (IL) and prelimbic (PrL) prefrontal cortex) only for the SP task. In contrast, a positive correlation

was found in a distinct set of brain regions (nucleus accumbens shell (AcbSh), AhiAl, ventral pallidum (VP)

and dorsomedial hypothalamic nucleus (DMD)) during the EsP and SxP tasks. Specifically, the VP exhibited

a very strong and highly significant linear correlation with RDI values during both the EsP and SxP tasks

(Fig 3G). These results suggest a link between stimulus-specific bias in $^\Delta$θP and behavioral preference in a

task-specific manner.

Figure 3. Stimulus- and task-specific LFP power changes during investigation bouts.

A. Heat maps of average theta power in AhiAl, before and during social investigation bouts of subjects
with social (above) and object (below) stimuli. Each row represents the mean Z-score of all bouts in a
single session (using 0.5 s bins). Time '0' represents the beginning of the bout. The color code scale is
on the right.
B. As in A, for investigation bouts of isolated (above) and grouped (below) social stimuli during EsP tasks.
C. As in A, for investigation bouts of female (above) and male (below) social stimuli during SxP tasks.
D. Mean (±SEM) Z-score trace of the data shown in A for both stimuli.
E. As in D. for the data shown in B.
F. As in D, for the data shown in C.
G. Correlation between mean change in theta power during investigation bouts ($^{\Delta}\theta$P) in specific brain
regions and RDI values during the various tasks. Only statistically significant linear correlations are
shown.
H. A 3D plot of the mean difference between preferred and less-preferred stimuli in $^{\Delta}\theta$P. Each dot
represents a given brain region, color- and shape-coded according to the combined bias across all
tasks.
I. As in B, for $^{\Delta}\gamma$P.
See also Fig. S4.
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To further explore this link, we plotted $^{\Delta}\theta$P bias across all tasks on a 3D plot, separately for each brain
region. We found that almost no region showed bias towards the object stimulus in the SP task, with the
various regions being equally distributed between the two stimuli in the EsP and SxP tasks (Fig. 4B). In
contrast, when $^{\Delta}\gamma$P was analyzed (Fig. 4C), we observed an opposite picture. Here, almost all brain regions
exhibited stronger responses to the grouped and male stimuli in the EsP and SxP tasks, yet were rather
equally distributed between the two stimuli in the SP task. Thus, for $^{\Delta}\gamma$P, most brain regions (14/18) were
equally divided between those biased towards less-preferred stimuli (i.e., object+grouped+male) and
those biased towards the type of stimulus used in all three tasks (i.e, social+grouped+male). The
probability of such an arrangement to occur by chance is smaller than 0.001 (1-binomial test) for each of
these two groups. The results thus suggest that a bias in gamma power is mostly associated with the
characteristics (i.e, valence or type) of the stimulus. They also generally demonstrate opposite stimulus-
dependent bias patterns between the theta and gamma rhythms during stimulus investigation, in contrast
to their significant correlation when measured during the entire encounter period (Fig. 2E-G). This implies
the existence of an independent active state in the social brain during stimulus investigation. Notably, of

all brain regions considered, the vDG stood out as the only region biased to the combination of

object/isolated/female stimuli. Moreover, this region showed an extreme bias for all these stimuli in both

$^{\Delta}\theta$P and $^{\Delta}\gamma$P. These results point to a unique position for the vDG in the social brain, as also supported by

results presented below.

Social encounters modulate coherence between brain regions in a social context-dependent manner

Synchronous activity (coherence) enhances effective communication between neuronal groups in

different brain regions and dynamically binds them into functional networks (Fries, 2015). We, therefore,

examined coherence in LFP signals between each pair of brain regions recorded by us, in both the theta

and gamma bands. During the baseline period, the mean theta coherence between all pairs of brain

regions (99 pairs) was similar across all tasks (Fig. 4A). Thus, the subjects displayed similar global brain

synchronization while exploring the arena without stimuli, in all tasks. However, the change in theta

coherence ($\Delta\theta$Co) measured during the encounter period differed significantly between tasks. While

almost all pairs of brain regions exhibited increased theta coherence during the SP task, we observed

significantly milder increases during EsP and SxP tasks, with many paired regions showing reduced

coherence (Fig. 4B, E-G). Similar relationships among tasks were observed for changes in gamma

coherence ($\Delta\gamma$Co), although here the general tendency was one of decreased coherence during the

encounter period (Fig. 4C-G). Notably, there was almost no correlation between the baseline period

coherence and the change in coherence during the encounter period for any task (apart a weak correlation

for SP gamma coherence; r=-0.21, p=0.0111; not shown). This suggests that the encounter-induced

coherence change represents an internal state, independent of the resting state. Finally, when calculating

the correlations across all paired regions in $\Delta\theta$Co between the various tasks, we found a statistically

significant high correlation between SxP and EsP, while no correlation was found between SP and SxP. A

milder but significant correlation was found between SP and ESP (Fig. 5H). In contrast, all correlations

were found significant for $\Delta\gamma$Co. These results suggest a gradual shift from SP to ESP and to SxP when in

$\Delta\theta$Co brain pattern is measured across the whole encounter.

Figure 4. Social encounters modulate the coherence between brain regions in a social context-
dependent manner.

A. Mean theta coherence during the five min-long baseline period before the encounter period for each
task, across all (n=99) pairs of brain regions recorded during all tasks (Kruskal-Wallis test, H = 0.75, *P* =
0.687).

B. As in A, for mean normalized change in theta coherence (ΔθCo) during the encounter period. Note the
significant difference between the SP and other tasks (****p<0.0001, Dunn's *post-hoc* test following
the main effect in a Kruskal-Wallis test).

C-D. As in A and B, for gamma coherence (***p<0.001, ****p<0.0001).

E. Color-coded matrix of the mean normalized ΔθCo (upper left) and ΔγCo (lower right) values for all pairs
of brain regions in the SP task. Empty spots represent brain region pairs with fewer than five recorded
sessions. Black spots separate between the ΔθCo and ΔγCo matrices.

F. As in E, for EsP.

G. As in E, for SxP.

H. Coefficients and significance of Pearson's correlations of ΔθCo across all coupled brain regions for each
pair of tasks (****p<0.0001).

I. As in H, for ΔγCo.

See also Fig. S5.

We, therefore, examined the encounter-induced coherence changes for each brain region separately, by
comparing the change in coherence between a given region and all other regions across tasks in the theta
(Fig. S5A) and gamma (Fig. S5B) bands. We found that differences between tasks were brain-region
specific, with most (13/18) regions showing significant differences between at least two tasks in ΔθCo and
almost half (8/18) showing differences in ΔγCo. Notably, in all cases, we found significantly higher
coherence changes during the SP task, as compared to at least one task, and in many cases, to both other
tasks. Thus, a subset of the recorded brain regions displayed differential changes in theta or gamma
coherence among the social contexts, with this change being majorly increased in the SP task, as
compared to the other two tasks.

Brain-wide coherence changes during investigation bouts reflect the social context

To explore possible modulation of coherence during investigation bouts, we calculated the mean $^\Delta$θCo
between each pair of brain regions during all investigation bouts towards a given stimulus, similarly to

how we analyzed power changes (Fig. 3). Since data had been collected for a large number of brain-region

pairs (overall, 99 pairs recorded across all tasks for at least 5 sessions per task), we focused on pairs with

a mean that crossed a cutoff value ± 1.5*standard deviation (SD) for each stimulus (about 20% of the

pairs). When plotting differences in $^\Delta\theta$Co between the two stimuli in each task on a 3D plot (Fig. S6A-B),

we observed a much wider distribution than was found for power (Fig. 3H-I), suggesting distinct principles

of distribution. To further explore this possibility, we examined all pairs of brain region that passed the

aforementioned threshold, separately for each stimulus (Fig. 5A). Surprisingly, the three stimuli of the

same type (i.e, social, grouped, male) did not share even a single pair of brain regions that passed the

$^\Delta\theta$Co cutoff value. Similarly, the preferred stimuli (i.e, social, isolated, female) also did not share even a

single pair among them. In contrast, multiple pairs of brain regions shared similar changes in theta

coherence between both stimuli used in each task (Fig. 5A). For example, CeA-PrL and MeAD-VP showed

increased coherence for both social and object stimuli, BLA-LS and EA-Acbc showed increased coherence

for both isolated and grouped stimuli and Pir-AcbC and EA-AcbC exhibited the strongest increase in theta

coherence for both male and female stimuli. Similar results were observed for gamma coherence (Fig.

S6C). Thus, changes in coherence seem to be dictated by the social context rather than by stimulus

characteristics, such as its type or valence.

For quantitative examination of this possibility, we calculated the correlation across all brain regions for

either $^\Delta\theta$Co (Fig. 5B) and $^\Delta\gamma$Co (Fig. 5C), between pairs of stimuli which share common context, type or

valence. We found strong and highly significant correlations between all pairs of stimuli used in the same

task (sharing context). In contrast, among the three stimuli of the same type, only grouped (ESP) and male

(SxP) showed significant correlation. Similarly, among preferred stimuli, only isolated (EsP) and female

(SxP) showed significant correlations. Notably, in both of these cases the correlation was weaker than the

correlation between any pair of stimuli sharing the same context (Fig. 5B). Similar results were found for

$^\Delta\gamma$Co (Fig. 5C). Thus, we conclude that the coherence changes in both theta and gamma rhythms during

stimulus investigation had the strongest association with the context of the social interaction, relative to

any characteristic of the stimulus.

Finally, we employed a Decision trees (multi-class Random forest) classifier to examine if $^\Delta\theta$Co and $^\Delta\gamma$Co

contain information which may be used to discriminate between the various contexts or stimuli. First, we

validated that the model achieved good (~60%) and significant accuracy in predicating the social stimulus

vs. object in the SP task using either $^\Delta\theta$Co or $^\Delta\gamma$Co. Notably, the classification of the object vs. social was

not accurate, suggesting that the presence of the social stimulus (social context) mask the object

classification (Fig. S7A-B). Then, we used the same model for predicting the social context and found that

using $^\Delta\theta$Co (Fig. 5D), but not $^\Delta\gamma$Co (Fig. 5E), allowed the model to predict the right context better than any

other context, and that this prediction was the only one achieving more than a chance level (33.3%)

accuracy (although only SxP classification got statistical significance). In contrast, the same model worked

poorly for predicting stimulus identity among all six stimuli (Fig. S7C-D). Using the LFP theta power ($^\Delta\theta$P)

for predicting the social context by the same model achieved good and significant classification only for

the SP (Fig. S7E), while using both theta power and coherence allowed accurate prediction of both SP and

SxP contexts (Fig. S7F). These results suggest that LFP rhythmicity in the theta range, especially the

coherence of between the various brain regions, is informative regarding the social context of the animal

more than regarding the identity or valence of the social stimuli.

Figure 5. Coherence changes during social investigation are informative regarding the social context

A. Distribution of changes in theta coherence during investigation bouts ($^\Delta\theta$Co) between each pair of brain regions, plotted separately for each stimulus used in the SP (blue), EsP (green) and SxP (red) tasks. The names of brain region pairs which passed the mean cutoff value ±1.5*SD are labeled, with those showing similar $^\Delta\theta$Co for both stimuli in the same task in bold.

B. Spearman's correlation coefficients of mean $^\Delta\theta$Co across all paired brain regions, for couples of stimuli which were either used in the same task (left, brown bars), of the same type (middle, gray) or having the same valence (right, yellow). The correlated two stimuli are denoted by asterisk below each bar, while the statistical significance of the correlation is marked above the bars.

C. As in B, for $^\Delta\gamma$Co.

D. A color-coded confusion matrix for a multi-class Random forest classifier employed for predicting the social context from $^\Delta\theta$Co values across all brain regions and stimuli. The scale of the accuracy's color code is shown to the right. The percentage of cases a label was predicted for each ground truth are marked in the middle of each spot. *p<0.05, **<0.01, Mann-Whitney test.

E. As in D, for $^\Delta\gamma$Co.

See also Figs. S5, S6.

Analysis of Granger causality suggests that specific brain regions serve as hubs

The coherent LFP rhythmicity in the social brain can be dominated by specific regions serving as hubs, thereby preceding other regions in terms of rhythmic neural activity. To identify hub candidate regions, we first selected brain regions which are statistically over-represented (see Methods) among pairs of regions exhibiting strong (mean ± 1.5*SD) bias in any task, separately for $^\Delta\theta$Co (Fig. 6A) and $^\Delta\gamma$Co (Fig. 6B). We then examined the dependence of LFP rhythmicity of each of these regions in terms of preceding rhythmicity of other regions by calculating the change in Granger causality (GC) (Barnett and Seth, 2014) during the encounter period (Fig. 6C-E). We found distinct patterns of statistically significant changes in GC (in the encounter vs. baseline periods) between the various tasks (Fig.6-H). Some regions, however, presented significant GC changes in all tasks, suggesting that they might function as hubs. For example, vDG and AcbC participated in significant GC changes in both theta and gamma rhythms in all tasks. At the same time, PrL and AhiAl were explicitly involved in theta GC changes in all tasks. Interestingly, theta GC changes from vDG to AhiAl increased during a SP task but decreased during a EsP task, while theta GC changes from PrL to vDG decreased during both EsP and SxP tasks. These results suggest that these brain regions dictate LFP rhythmicity in the social brain during social investigation.

Figure 6. Distinct patterns of changes in Granger causality during the encounter period among tasks.

A. Schematic representation of the brain regions over-represented among the brain region pairs that

exhibited strong (mean ± 1.5*SD) theta coherence bias towards one of the stimuli in any task. The

regions are color-coded according to the task in which they were over-represented.

B. As in A, for gamma coherence.

C. Schematic representation of significant changes (in encounter vs. baseline periods) in theta band GC

during a SP task, among the regions listed in A. The direction of the GC changes in shown by a black

arrow (top to bottom on the right and bottom to top on the left).

D. As in C, for EsP.

E. AS in C, for SxP.

F-H. As in C-E, for gamma band

Context-specific synchronization of LFP rhythmicity in the ventral dentate gyrus with precise behavioral

events

To further examine the candidate hub regions, we exploited our ability to determine the exact timing of

each investigation bout to quantify the synchronized modulation of LFP rhythmicity, relative to these

events. Thus, we compared the modulation of theta and gamma power in all regions associated with

significant GC changes (Fig. 6) relative to a defined battery of specific behavioral events (Fig. 7A). These

events included the beginning and end of short (<2 s) and long (>2 s) investigation bouts towards specific

stimuli, as well as transitions between stimuli. We found a main effect in ANOVA for multiple events,

although in most cases, none of the regions showed significance *in post-hoc* analysis (see Table S2). One

region, the vDG, did, however, exhibit significant differences between events. The vDG displayed

significantly higher theta and gamma powers at the end of long investigation bouts of social stimuli, as

compared to object stimuli, specifically in the SP task (Fig. 7B-G and S7A-B). The same region also exhibited

decreased theta and gamma powers at the beginning of transitions from isolated to grouped stimuli, as

compared to non-transitional bouts, specifically in the EsP task (Fig. 7H-M and S7C-D).

Figure 7. Context-specific differences in vDG LFP rhythmicity in specific behavioral events

A. Color-coded scheme of specific behavior event types, with ↓ indicating the beginning of an event, ⊥ indicating the end of the event and ***** indicating the beginning of event after transition. Events showing significant differences in vDG LFP power are highlighted in yellow.

B. Super-imposed traces of the mean (±SEM) Z-score of changes in vDG theta power at the end of long bouts towards either a social stimulus (pink) or an object stimulus (purple) in the SP task. Time 0 represents the end of the bout, while the 5 s period before time 0 was considered as baseline. *$p<0.05$, according to Student's t-test between the mean Z-score values averaged over the last 2 s of the traces.

C. As in B, for gamma power in the vDG during SP tasks.

D-E. As in B-C, for the EsP task.

F-G. as in B-C, for the SxP task.

H-I. As in B-C, for changes in LFP power at the beginning of transitional vs. non-transitional investigation bouts of social and object stimuli across SP task sessions.

 J-K. As in H-I, for the EsP task. **$p<0.01$ by a Mann-Whitney test following the main effect in ANOVA.

L-M. As in H-I, for the SxP task.

See also Fig. S8.

These results, together with those shown in Fig. 3B-C and Fig. 6, suggest that the vDG functions as a hub in the social brain network by dictating the rhythmic neural activity of the network in a social context-dependent manner. In accordance with this idea, a descriptive plot of the change in theta and gamma coherence during investigation bouts between the vDG and all other regions reveals a pattern which is highly stimulus- and social context-dependent (Fig. 8).

Figure 8. Stimulus- and social context-dependent patterns of coherence changes between the vDG and other brain regions

A. Color-coded flower plots of the change in theta ($^{\Delta}\theta$Co, upper plot) and gamma ($^{\Delta}\gamma$Co, lower plot) coherence during investigation bouts made in the course of SP sessions towards the preferred (blank leaves) and less-preferred (dashed leaves), between the vDG and all other regions simultaneously recorded with it during at least five sessions across all tasks.

B. As in A, for EsP sessions.

C. As in A, for SxP sessions.

Discussion

In this study, we used multi-site electrophysiological recordings from the murine social brain to seek system-level neural correlates of three distinct aspects of social interaction, namely, the identity of the social stimulus, its relative valence (preference) and the social context. To distinguish between these three aspects, we relied on three social discrimination tasks (i.e., SP, EsP, and SxP) in which male mice clearly prefer one of two distinct stimuli. This design enabled us to employ the same type of social stimulus, a novel group-housed male mouse, in all three tasks, with this stimulus being the preferred stimulus in the SP task and the less-preferred stimulus in the other two tasks. Importantly, all three tasks took place in the same experimental arena, which enables uniform interactions between the subject and the stimuli, i.e., stimulus investigation by the subject (Netser et al., 2019). Consequently, as much as we could measure, subject behavior was almost identical in all three tasks. Therefore, behavioral differences cannot explain the significant differences in the patterns of rhythmic LFP signals observed among the different tasks.

We analyzed LFP signals at three different time resolutions, specifically, across the session, during investigation bouts, and during specific behavioral events, such as at the beginning and end of long or short investigation bouts. When analyzing the power of both theta and gamma rhythms over an entire session, some aspects seemed to be dictated by a general state of arousal. In accordance with previous studies by us and others (Kuga et al., 2022; Tendler and Wagner, 2015), virtually all brain regions exhibited higher level of theta and gamma power during the encounter period, as compared to the baseline period. Our observation that the level of enhanced power was both brain region- and task-specific strongly suggests that this was not caused by enhanced electrical noise or any other artifact but rather by a genuine internal state of the animal. The uniform dynamics of both theta and gamma power changes across all brain regions and tasks during the encounter period further supports the existence of an internal arousal changes which are independent of behavioral dynamics or context. Notably, we observed significant correlations across brain regions between theta and gamma power changes in all tasks, suggesting that both rhythms are similarly influenced by the internal state. In agreement with our previous studies in both rats and mice (John et al., 2022; Tendler and Wagner, 2015), theta and gamma power maintained their high levels for a time, even after removal of the stimuli from the arena (not shown), further supporting the presence of an internal state of arousal, which slowly fades away. This state did not seem to be induced by subject movement, as we found no correlation between subject speed and changes in theta or gamma power for any brain region.

While the dynamics of the internal arousal state seemed to be similar across the distinct contexts, other

aspects of the general (session-wise) changes in theta and gamma power exhibited context-specific

characteristics. For example, the general changes in both power and coherence were highest in the SP

task, suggesting a higher level of arousal. These results are somewhat surprising, given how the SP task

involved only one social stimulus and assuming that among the various stimuli tested, the female would

be the most attractive to the male subjects. Our interpretation is that the SP task is simpler in terms of

conflicting tendencies, as it requires the animal to choose between an inanimate object and a conspecific,

while the other two tasks involve two conspecifics, thereby presenting the subject with a more challenging

dilemma. The higher confidence of the subject during the SP task is in accord with the simpler pattern of

theta coherence changes observed during this task (seen as a general increase across almost all brain

region pairs). Overall, these suggests that the arousal level may distinguish between some contexts, which

is in accordance with the ability of the Random Forest model to predict only the SP context based on the

arousal-induced LFP power. Nevertheless, the changes in theta and gamma power across the encounter

period did not differ between the EsP and SxP tasks, and thus cannot be the sole basis for the context-

specific responses to social cues.

Notably, a recent paper (Mague et al., 2022) that employed similar recordings during the SP test, used the

power, coherence and GC data (termed *Electome network*) from various regions of the social brain in a

machine-learning model to discriminate between social and object investigation. In accordance with our

results, this study reported that the model's precision was higher for the social than for the object, thus

suggesting that the social stimulus masks the object, which may be attributed to the social context.

Analysis of the power change, specifically during stimulus investigation bouts, yielded a different picture

than did session-wide analysis. First, we found no correlation between theta and gamma power changes

during these periods, suggesting a distinct state of active sensing which characterizes stimulus

investigation. Moreover, although both theta and gamma power changes across brain regions showed

bias to specific combinations of stimuli, they did so in distinct manners. While theta power was biased

towards the preferred stimulus in the SP task, with almost no region (other than hippocampal areas)

showing a preference for object stimuli, the gamma power was clearly biased towards the less-preferred

stimuli in the ESP and SxP tasks (grouped and male stimuli), while showing a mixed preference between

stimuli in the SP task. Thus, as related to gamma power, the social brain seems to be divided between

regions associated with the valence of stimulus (biased towards less-preferred stimuli) and brain regions

associated with the type of stimulus. It should be noted that theta rhythmicity is thought to reflect top-

down processes, such as arousal and attention (Colgin, 2011; Gordon, 2011; Harris and Gordon, 2015b),

which are regulated by brain wide-active neuromodulators and recruit distributed brain networks
(Clayton et al., 2015; Fiebelkorn and Kastner, 2019; Helfrich et al., 2019; Karakas, 2020; Knyazev, 2007).
In contrast, gamma rhythmicity is considered a bottom-up process (Buzsaki and Wang, 2012; Headley and
Pare, 2013), associated with the synchrony of local inhibitory networks (Benchenane et al., 2011; Buzsaki
and Wang, 2012; Headley and Pare, 2013; Palva and Palva, 2018). This distinction may explain why theta
and gamma rhythms reflect stimulus characteristics in an opposing manner.

In accordance with our hypothesis, that coherent theta and gamma rhythms couple various regions of the
social brain in a social context-dependent manner, we found that the correlation in the coherence change
during stimulus investigation was strongest between the two stimuli in each task, even the EsP and SxP
tasks. In contrast, there were weaker correlations, if any, among the three stimuli of the same type (social,
grouped, male) or the preferred stimuli (social, isolated, female). The fact that the same correlation
pattern was observed for both theta and gamma coherence supports the validity and significance of the
observation. Moreover, using a Decision Tree classifier, we demonstrated that the theta coherence
between the recorded areas could generate predictions regarding the social context, but not the specific
stimulus, which are accurate above the chance level. The limited accuracy of the model may be attributed
to the restricted number of recorded regions. Thus, we expect that a more comprehensive analysis of the
coherence within the social brain will be able to generate highly accurate prediction of the social context.
Moreover, GC analysis, representing causal time relationships between various brain regions, also
suggests distinct patterns of changes across the various contexts. Altogether, these results support the
idea that the social brain processes information during stimulus investigation in a context-dependent
manner dictated by the context-dependent pattern of coherence within the network. Such a mechanism
may explain how the same stimulus induces distinct patterns of brain activity in different social contexts,
which then elicits distinct behavioral responses to a stimulus.

Finally, the coherence change and GC analyses led us to identify a small subset of brain regions that seem
to highly influence the network during the various tasks. Of these, the vDG and AcbC were involved in
significant GC changes during all tasks in both the theta and gamma bands, and thus may serve as hubs
that dictate the activities of other regions. Analysis of LFP power in relation to a battery of specific
behavioral events demonstrated that while the small group of brain regions considered showed
differential responses as a whole, the vDG was the only region that alone showed statistically significant
responses. Together with its strong bias towards specific stimuli, as demonstrated for both theta and
gamma power during investigation bouts (Fig. 4B-C), these results suggest a unique and central role for
the vDG in orchestrating neural activity across the social brain during social behavior. This conclusion

agrees with previous studies reporting a central role of the dentate gyrus in social behavior, in general

(Cai et al., 2018; Doucette et al., 2020; Leung et al., 2018), and specifically, in social discrimination (Cope

et al., 2020; Li et al., 2022). Notably, multiple studies have implicated the DG in coding contextual changes.

For example, DG neurons were shown to rapidly detect and encode contextual changes (Leutgeb et al.,

2007), while a knockout mouse for NMDA receptors specifically in DG granule cells abolished the ability

of the mutant mice to distinguish between two similar contexts (McHugh et al., 2007). Moreover,

hypothalamic supramammillary neurons projecting to the DG were shown to be activated by contextual

novelty (Chen et al., 2020), while the activity of ventral hippocampal neurons was shown to process

information in a social context-sensitive manner (Wu et al., 2023). These studies are thus in line with our

findings regarding the involvement of the vDG in dominating context-dependent social behavior.

In conclusion, our results suggest that the distribution of LFP rhythmic activity in the social brain and, most

specifically, coherence between the various regions, which is dictated by the vDG, is context-specific and

may thus mediate context-specific processing of social information, leading to social context-dependent

social responses and behavior.

Methods

<u>Animals</u>

Adult male and female CD1 mice (12-14 weeks old) were acquired from Invigo (Rehovot, Israel). All mice

were housed in groups of 3-5 in a dark/light 12-hour cycle with *ad libitum* food and water. Following

surgery, implanted mice were housed in isolation so as to not disturb the implanted EAr. Experiments

were performed in the dark phase of the dark/light cycle in a sound- and electromagnetic noise-

attenuated chamber. All experiments were approved by the Institutional Animal Care and Use Committee

of the University of Haifa (Ethical approval #616/19).

<u>Surgery</u>

Mice were anesthetized using isoflurane (induction 3%, 0.5%-0.8% maintenance in 200mL/min of air;

SomnoSuite) and placed over a custom-made heating pad (37°C) in a standard stereotaxic device (Kopf

Instruments, Tujunga, CA). Two burr holes were drilled for placing the ground and reference wires (silver

wire, 127 µm, 300-500 Ω; A-M Systems, Carlsborg, WA). Two watch screws (0-80, 1/16", M1.4) were

inserted into the temporal bone. The coordinates for Prl (AP= 2mm, ML= -0.3, DV= -1.8), AcbC (AP= 1, ML=

-2.3, DV= -4.7), Pir (AP= -2, ML= -3.3, DV = -5) and CA1 (AP= -3, ML= -3.3, DV = -4.7) were indicated over

the left hemisphere using a marker. The skull covering these marked coordinates was removed using a

dental drill, and the exposed brain was kept moist with cold, sterile saline. We custom-designed the EA

(Mohapatra et al., 2022) from 16 individual 50 µm formvar-insulated tungsten wires (50-150 kΩ,

#CFW2032882; California Wire Company). Before implantation, the EAr was dipped in DiI (1,1'-

Dioctadecyl-3,3,3',3'-tetramethylindocarbocyanine perchlorate; 42364, Sigma-Aldrich) to visualize

electrode locations *post-mortem*. The reference and ground wires were inserted into their respective burr

holes. The EAr was lowered onto the surface of the exposed brain using a motorized manipulator (MP200;

Sutter instruments). The dorsoventral coordinates were marked using the depth of the electrode targeting

the PVN (AP= -1 mm, ML= -0.3), which was lowered slowly to -4.7 mm. The EA and exposed skull with the

screws were secured with dental cement (Enamel plus, Micerium). Mice were sub-cutaneously injected

with Baytril (5mg/kg; Bayer) and Norocarp (5 mg/kg; Carprofen, Norbrook Lab) post-surgery and allowed

to recover for three days.

<u>Electrophysiological and video recordings</u>

Following brief exposure to isoflurane, subjects were attached to the headstage (RHD 32 ch, #C3314, Intan

Technologies) through a custom-made Omnetics to Mill-Max adaptor (Mill-Max model 852-10-100-10-

001000). Behavior was recorded using a monochromatic camera (30 Hz, Flea3 USB3, Flir) placed above

the arena. Electrophysiological recordings were made with the RHD2000 evaluation system using an ultra-

thin SPI interface cable connected to the headstage board (RHD 16ch, #C3334, Intan Technologies).

Electrophysiological recordings (sampled at 20 kHz) were synchronized with recorded video using a TTL

trigger pulse and by recording camera frame strobes.

Experiment design

We recorded the behavior and neural activity of 14 males in the SP task, 13 males in the ESP task, and 11

males in the SxP task (Table S1), while targeting 18 distinct brain regions. All the stimuli used for the tasks

were unfamiliar to the subject mice. In experiments, the mice were briefly exposed to isoflurane, and the

EAr was connected to the evaluation system. After 10 minutes of habituation, the recordings started in

the arena (30 x 22 x 35 cm) with empty triangular chambers (12 cm isosceles, 35 cm height), as previously

described (Netser et al., 2019). The triangular chambers had one face ending with metal mesh (18 mm x

6 cm; 1 cm x 1 cm holes) through which the mice interacted with the stimuli. The test was divided into

two 5 min periods, a baseline period (pre-encounter) and a period of encounter with the stimuli. The

stimuli for the SP task were a novel group-housed male mouse (social) and a Lego toy (object). For the ESP

task, isolated (7-14 days) male and group-housed male mice served as stimuli. Finally, for the SxP task,

group-housed male and female mice were used as stimuli. Each subject was evaluated for three sessions

of each task. We excluded sessions from further evaluations when there was either removal of the

headstage from the EA by subjects or video recording from a session was missing, which accounts for the

unequal number of sessions and subjects across tasks.

Histology

Subjects were transcardially perfused, and their brains was kept cold in 4% paraformaldehyde for 48 h.

Brains were sectioned (50 µm) horizontally (VT 1200s, Leica). Electrode marks were visualized (DiI coated,

Red) against DAPI-stained sections with an epifluorescence microscope (Ti2 eclipse, Nikon). The marks

were used to locate the respective brain regions, based on the mouse atlas.

Behavioral analysis

Subject behavior was tracked using the TrackRodent algorithm (Netser et al., 2019) for tethered mice.

Further parameters of behavior, like duration of interaction, interaction bouts, distance traveled by the

subjects, subject speed, transitions between stimuli, and RDI values were calculated from the tracked

results with custom codes written in MATLAB 2020a.

Electrophysiological data analysis

Only brain regions recorded for more than 5 sessions across at least 3 mice were analyzed. All signals were

analyzed with codes custom-written in MATLAB 2020a. First, the signals were down-sampled to 5 kHz and

low-pass filtered to 300 Hz using a Butterworth filter. The power and time for the different frequencies

were estimated using the 'spectrogram' function in MATLAB with the following parameters: Discrete

prolate spheroidal sequences (dpss) window = 2 s; overlap = 50% ; increments = 0.5 Hz; and time bins =

0.5 s. The power of each frequency band (theta: 4-12 Hz and gamma: 30-80 Hz) was averaged for both

the baseline and encounter periods. Change in theta (ΔθP) and gamma (ΔγP) powers for each brain region

were defined as the mean difference in power between the encounter and baseline periods (Fig. 2C-D, H-

I). We calculated $^{\Delta}$θP and $^{\Delta}$γP throughout each investigation bout for a stimulus using Z-score analysis,

where the pre-bout 5 s period served as baseline. Furthermore, for each task, we averaged the Z-score

across all bouts with the same stimulus in each session and compared these between the two stimuli (Fig.

8, S6 and S3). LFP power ($^{\Delta}$θP and $^{\Delta}$γP) for specific bouts with each stimulus was estimated by calculating

the difference between the average power per second during an investigation bout (which was longer

than 2 s) during the encounter period and the average power per second for investigation of both empty

chambers in the baseline period of the same session, followed by averaging these values over all sessions

(Fig. 4).

Coherence analysis

We used the 'mscohere' function of MATLAB to estimate coherence values using Welch's overlapped

averaged periodogram method. The magnitude-squared coherence between two signals, x, and y, was

defined as follows:

641
$$Coherence_{xy} = \frac{S_{xy}}{\sqrt{S_{xx} S_{yy}}}$$

where S_{xy} is the cross-power spectral density of x and y, S_{xx} is the power spectral density of x and S_{yy} is

the power spectral density of y. All coherence analysis was quantified between brain regions pairs

involved in at least five sessions of behavior tasks. Coherence for the baseline period was quantified as

the average coherence of all brain region pairs for each context (Fig. 5A and F). Changes in coherence

(ΔθCo and ΔγCo) during the encounter period (Fig. 5B and G) between a pair of brain regions were

calculated as follows:

$$Change\ in\ Coherence = \frac{\mu\ (Coherence_{encounter} - Coherence_{baseline})}{\sigma\ (Coherence_{encounter} - Coherence_{baseline})}$$

where, $Coherence_{encounter}$ is the absolute coherence value between a pair of regions within a frequency

band during whole encounter period. $Coherence_{baseline}$ is the absolute coherence value between a pair of

regions within a frequency band during an entire encounter period. The change in coherence for specific

bouts ($^{\Delta}$θCo and $^{\Delta}$γCo) to each stimulus was estimated by calculating the difference between the average

coherence per second during an investigation bout (≥2 s) in the encounter period and the average

coherence per second for investigation with both empty chambers during the baseline period of the same

session, followed by averaging these values over all sessions (Fig. 6A and S5C). Brain regions that displayed

higher frequencies of crossing the threshold of mean ± 1.5 SD $^{\Delta}$θCo and $^{\Delta}$γCo, based on a binomial

distribution test, were considered to be hubs in the coherent social brain (Fig. 7A-B).

<u>Assessing inter-regional pairwise conditional Granger causality</u>

We employed the multi-variate GC toolbox (Barnett and Seth, 2014) to calculate GC values separately for

baseline and encounter periods between brain regions separately for each task and rhythm. To this end,

we selected brain regions most represented among brain region pairs that crossed the mean ± 1.5*SD

threshold for the difference in coherence change between preferred and less preferred stimuli in any task,

separately for $^{\Delta}$θCo and $^{\Delta}$γCo. For GC analysis, LFP signals were measured at a reduced sampling rate of

500 Hz. We used the "tsdata_to_infocrit" function to determine the model order of the vector

autoregressive (VAR) model. The median model order for all three tasks was 38 (Bayesian information

criterion). To further fit the VAR model to our multi-session, multivariate LFP data, the "tsdata_to_var"

function of LWR (Levinson-Whittle recursion) in the regression mode and a median model order of 38 was

used separately for the baseline and encounter periods of each task. Next, we estimated the

autocovariance sequence of the fitted VAR model with the "var_to_autocov" function. To maximize the

computational efficiency of the function, an acmaxlags of 1500 was chosen. This process did not violate

the autocovariance VAR model, as was estimated by the "var_info" function. Finally, we calculated the

pairwise conditional frequency-domain multivariate GC matrix using the "autocov_to_spwcgc" function,

and summed the GC for the relevant frequency band (theta or famma) using the "smvgc_to_mvgc"

function.

<u>Assessing neural responses to behavioral events</u>

We divided all investigation bouts into specific behavioral events, such as the start and end of an

investigation bout or transition from one stimulus to the other (Fig. 7A, nine distinct types). We aligned

LFP power and behavior events for each stimulus by calculating mean power 5 s before and 5 s after the

beginning (or end) of all investigation bouts (0.5 s bins) in a session. Furthermore, for each bout, the mean

power was normalized using Z-score analysis, where a pre-bout duration of 5 s served as baseline (Table

S2).

<u>Statistical analysis</u>

Statistical analysis was performed using GraphPad Prism 9.5. To test for normal distribution of the data,

we used the Kolmogorov-Smirnov and Shapiro-Wilk tests. Table S3 summarizes the specific tests

conducted for each figure. A paired t-test or Wilcoxon matched-pairs signed rank test was used to

compare different stimuli or conditions for the same group. An unpaired t-test or Mann-Whitney test was

performed to compare a parameter between distinct groups. For comparison among multiple groups and

parameters, ANOVA (normal distribution), Welch's ANOVA (assuming unequal variance), and Kruskal-

Wallis test (non-normal distribution) were applied to the data. If a main effect or interaction were found

in the tests above, Šídák's test, Dunnett's T3 test or Dunn's *post-hoc* multiple comparison corrections were

applied. Repeated measures ANOVA or a Friedman test was used to compare multiple groups and

parameters with repeated variables. When main effects were observed in above tests, Šídák's or Dunn's

test were used for multiple comparisons corrections, respectively. Additionally, for comparison of two

factors and the interaction between them, from multiple groups and parameters where one of the factors

has repeated measurements, was performed using two-way ANOVA (no missing variables) or mixed-

models ANOVA (Restricted maximum likelihood model, REML). The ANOVA tests were followed by Šídák's

multiple comparison test if main effects or interactions were found. The association between two groups

or parameters was compared with either Pearson's or Spearman's tests. A binomial distribution test was

performed to compare the probability of brain regions representing above-chance levels for specific

parameters.

<u>Decision tree classifier model</u>

707 **Data normalization – subtracting the mean value for each brain regions pair per mouse:** The data from

708 two mice (total 14) were ignored as they had less than 40 recorded brain regions pairs (out of 99). The

709 mean value of each pair was computed and subtracted for each mouse separately. This helped to reduce

710 the variability of the measurements across mice and improved classification accuracy. To reduce over-

711 representation of a single stimulus in the computation of the mean value for a pair, we first averaged the

712 mean value per stimulus (for a specific mouse) and then subtracted the average of these means.

713 **Averaging bouts:** The average bout for each stimulus was computed for each session.

714 **Data Imputation:** For each mouse, a slightly different set of brain areas were recorded due to slight

715 inaccuracies in placing the electrodes and slight difference in the individual mouse anatomy. This resulted

716 in missing entries from some of the brain regions pairs. We used a data imputation strategy to restore

717 these missing entries. Note that before this step, we subtracted the mean value per brain region per

718 mouse and averaged all the bouts from the same stimuli of the same session. The imputation algorithm

719 is based on the MICE algorithm (Azur et al., 2011). It is an iterative algorithm. In each iteration, it estimates

720 the missing entries by a linear combination of (some of) the other entries. The used data imputation

721 algorithm was defined as follows:

1. For each missing value of brain pair i in bout b, ($bp_{i,b}$), replace $bp_{i,b}$ with the average value of bp_i across the valid values bp_i (from all bouts of all mice with a valid measurement of bp_i).

2. For each bp_i ($order\ of\ brain\ pairs\ is\ randomized$):

 a. Randomly choose a set of predicting brain pairs $\{bp_j\}$ such that $bp_i \notin \{bp_j\}$ and $|\{bp_j\}| <$ 0.5*number_of_equations. Where the number_of_equations equals to the number of (averaged) bouts from all the mice (66 predicting brain pairs as the number of bouts in our dataset is 131 average bouts).

 b. Compute linear regression coefficients {aj} (by least square method) to minimize:

$$\underset{\{a_j\}}{\operatorname{argmin}} \sum_b \left(bp_{i,b} - \left(a_0 + \sum_j a_j bp_{j,b} \right) \right)^2$$

 c. For each bout b in which $bp_{i,b}$ was not measured in-vivo, replace it with its estimation: $a_0 + \sum_j a_j bp_{j,b}$

3. Repeat steps 2 for 20 iterations.

Code was implemented in Matlab 2021a.

737 **Classification and computation of confusion matrixes:** We used Matlab's *TreeBagger()* function to train

738 a multi-class Random forest classifier for discriminating between a pair of stimuli (social vs object) or

contexts (3 classes) or between stimuli (6 classes) or between. We used 80 random trees (a parameter of

the TreeBagger function). We used cross-validation with "one mouse leave out" strategy to compute a

confusion matrix for each mouse based on a training set that includes examples from all of the other mice.

We balanced the training set to have the same number of examples from each class by randomly removing

some of the training examples. Since both the balancing and the Random forest algorithm have a random

component, we repeated the estimation of confusion matrixes 100 times (for each mouse) to better

estimate the confusion matrixes. We then summed up all of the confusion matrixes (totally 1200

confusion matrixes: 12 mice and 100 confusion matrixes per mouse) and computed for each pair of classes

(i,j) the percent of cases where the prediction was i for bouts of class j.

Statistical Analysis: To compute p-values, we used the average (over 100 iterations) confusion matrix for

each mouse (totally 12 confusion matrixes in which each cell i,j represents the % of predictions of class i

for bouts of class j) and compare those with a set of random confusion matrixes which were generated by

the same procedure except for replacing the trained classifier with a random classifier. This random

classifier generated random labels with uniform distribution. To better describe the distribution of the

random confusion matrixes, we generated 83 random confusion matrixes per mouse (each one of them

is an average of 100 confusion matrixes). Then, the p-value for each cell in the confusion matrix was

computed separately by comparing the 12 values from the confusion matrix of the trained classifier to the

83*12=996 values from the confusion matrixes of the random classifier using Mann-Whitney U test. In

case a mouse did not have a bout from a specific class, this mouse was ignored in the computation of the

p-value for the cells of this ground truth class.

Declarations

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<u>Author contributions</u>

A.N.M.: Formal analysis, Investigation, Methodology, Validation, Visualization, Writing - original draft, and

Writing - review & editing; D.P.: Formal analysis, and software.; S.N.: Data curation, Project

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S.W.: Conceptualization, Funding acquisition, Project administration, Resources, Supervision, Writing -

original draft, and Writing - review & editing.

<u>Declaration of interests</u>

The authors declare no competing interests.

Supplementary figures

Figure S1: The electrode array and PSD profiles from individual sessions

A. Macro-view of the electrode array

B. Brain sections from mice with DiI-mediated electrode tip marks (red) in the targeted regions overlaid

on an atlas image of a similar DV plane. Left section = -2.36 mm from Bregma, right section = -4.72

mm, scale = 1 mm

C. The power spectral density (PSD) plots of LFP signals recorded in the MeAD, IL, PrL, CA1, AcbC, and

AcbSh during the encounter period of SP (left), EsP (middle) and SxP (right) task single sessions, all

conducted by the same mouse. The inset shows the PSD plots for 0-20 Hz band at higher resolution.

Figure S2. Similar dynamics of theta and gamma power across the various tasks and brain regions

A. Mean traces of ΔθP (left column) and ΔγP (right column) across all sessions of the SP task for each

brain region. The colored bar represents the encounter period.

B. As in A, for the EsP task

C. As in A, for the SxP task

D. Mean (±SEM) ΔθP, averaged across all brain regions for every minute of the baseline and encounters

periods of the SP task. Time 0 min represents the time of stimuli insertion. Lines below the bars

represent a significant difference between the first minute of the encounter and every minute of the

baseline period.

E. As in D, for the EsP task.

F. As in D, for the SxP task

G-I, as in D-F, for ΔγP.

Figure S3. No correlation exists between theta and gamma power changes during social encounters

and subject speed

A. Correlation coefficients across all SP task sessions for calculating Pearson's correlation between the

change in theta power (ΔθP) and the mean speed of the subject.

B. As in A, for EsP sessions.

C. As in A, for SxP sessions.

D-F. As in A-C, for gamma power (ΔγP).

Figure S4. Z-score analysis of changes in gamma power during social investigation of specific stimuli

A. Heat maps of average gamma power in AhiAl, before and during social investigation bouts of subjects with social (above) and object (below) stimuli. Each row represents the mean Z-score of all bouts in a single session (using 0.5 s bins). Time '0' represents the beginning of the bout. The color code scale is on the right.

B. As in A, for investigation bouts of isolated (above) and grouped (below) social stimuli during EsP tasks.

C. As in A, for investigation bouts of female (above) and male (below) social stimuli during SxP tasks.

D. Mean (±SEM) Z-score trace of the data shown in A for both stimuli.

E. As in D. for the data shown in B.

F. As in D, for the data shown in C.

Figure S5. Coherence changes during the encounter period of the various tasks are brain region-specific

A. Mean change in theta coherence (ΔθCo) between a given brain region and all other simultaneously

recorded regions during the encounter period, compared across the three tasks.

B. As in A, for gamma coherence (ΔγCo).

*$p<0.05$, **$p<0.01$, ***$p<0.001$, ****$p<0.0001$, Dunnett's and Dunn's *post-hoc* test following the main

effect in ANOVA and Kruskal Wallis test, respectively.

Figure S6. Distribution of theta and gamma coherence changes during social investigation bouts across

tasks

A. A 3D representation of the mean difference in theta coherence change during investigation bouts

($^\Delta\theta$Co) between the preferred and less-preferred stimuli, across all tasks. Each dot represents a pair

of brain regions (n = 84 pairs), color- and shape-coded according to the combined bias across all tasks.

Only pairs which showed a coherence change of 1.5*SD from the mean are presented. We excluded

any pair with fewer than five sessions of investigation bouts with one of the stimuli or with both.

B. As in A, for gamma coherence change ($^\Delta\gamma$Co)

C. Distribution of gamma coherence change ($^\Delta\gamma$Co) between each pair of brain regions during

investigation bouts, plotted separately for each stimulus used in the SP (blue), EsP (green) and SxP

(red) tasks. The brain region pairs which passed the mean ± 1.5*SD cutoff are labeled and those that

are shared by both stimuli in the same task are denoted in bold.

Figure S7. Random forest model can predict the social stimulus in the SP task but not the specific

stimulus among all six stimuli

A. A color-coded confusion matrix of a multi-class Random Forest classifier using the changes in

theta coherence during investigation bouts across the SP task to predict the type of investigated

stimulus among the two possible stimuli (social and object).

B. As in A, for gamma coherence.

C. A color-coded confusion matrix of the same model using the changes in theta coherence during

investigation bouts across all tasks to predict the type of investigated stimulus among the six

possible stimuli.

D. As in C, for gamma coherence.

E. A color-coded confusion matrix for the Random Forest classifier employed for predicting the social

context from $^{\Delta}\theta P$ values across all brain regions and stimuli. The scale of the accuracy's color code

is shown to the right. The percentage of cases a label was predicted for each ground truth are

marked in the middle of each spot. $*p<0.05$, $**<0.01$, $***<0.001$, $****<0.0001$, Mann-Whitney

test.

F. As in E, for the combination of $^{\Delta}\theta P$ and $^{\Delta}\theta Co$. $*p<0.05$, $**<0.01$, Mann-Whitney test.

Figure S8. Significant difference in gamma and theta power in specific behavioral events

A. Mean (±SEM) Z-score values of gamma power change in the vDG at the end of long (>3 s) investigation bouts towards social (pink) and object (blue) stimuli during SP task sessions, shown for three brain regions where significant changes in GC were found in the gamma band.

B.   Heat maps of male vDG gamma power changes before and during long (>3 s) investigation bouts

towards the social (above) and object (below) stimuli across all SP task sessions. Each row represents

the mean Z-score of all bouts in a single session (bins of 0.5s). Time point **'0'** represents the beginning

of the bout. The color code is on the r

C-D. As in A-B, for changes in theta power at the beginning of transitional vs. non-transitional

investigation bouts of grouped social stimuli across EsP sessions.

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