Brain Metabolic Network Covariance and Aging in a Mouse Model of Alzheimer's Disease

EJ Chumin[1,2,3], C Burton[1], R Silvola[4,5], SC. Persohn[1], M Veronese[6,7], and PR Territo*[1,4]

Affiliations:

[1] Stark Neurosciences Research Institute, Indiana University School of Medicine, Indianapolis IN 46202

USA

[2] Department of Psychological and Brain Sciences, Indiana University, Bloomington IN 47405

[3] Indiana University Network Science Institute, Indiana University, Bloomington, IN 47405

[4] Department of Medicine, Division of Clinical Pharmacology, Indiana University School of Medicine,

Indianapolis IN 46202 USA

[5] Eli Lilly and Company, Indianapolis IN 46202 USA

[6] Department of Information Engineering, University of Padua, Padua 35100 ITA

[7] Department of Neuroimaging, King's College London, London SE5 8AF UK

*Corresponding Author:

Paul R. Territo, PhD

1345 West 16th Street, BRTC 308

Indianapolis, IN 46202

pterrito@iu.edu

(317) 278-6230

Short Title: Metabolic Connectivity in Alzheimer's disease.

ABSTRACT

INTRODUCTION: Alzheimer's disease (AD), the leading cause of dementia worldwide, represents a human and financial impact for which few effective drugs exist to treat the disease. Advances in molecular imaging have enabled assessment of cerebral glycolytic metabolism, and network modeling of brain region have linked to alterations in metabolic activity to AD stage. **METHODS:** We performed ^{18}F-FDG Positron Emission Tomography (PET) imaging in 4, 6, and 12 month old 5XFAD and littermate controls (WT) of both sexes, and analyzed region data via brain metabolic covariance analysis. **RESULTS:** 5XFAD model mice show age related changes glucose uptake relative to WT mice. Analysis of community structure of covariance networks was different across age and sex, with a disruption of metabolic coupling in the 5XFAD model. **DISCUSSION:** The current study replicates clinical AD findings and indicates that metabolic network covariance modeling provides a translational tool to assess disease progression in AD models.

RESEARCH IN CONTEXT

SYSTEMATIC REVIEW: The authors extensively reviewed literature (e.g., PubMed), meeting abstracts, and presentations on approaches to evaluate brain network analysis in animal models. Based on the available data, there were clear gaps in our understanding of how metabolic networks change with disease progression at the preclinical phase, thus limiting the utility of these measures for clinical comparison in Alzheimer's disease (AD).

INTERPRETATION: Our findings indicate that employing metabolic covariance modeling in mouse models of AD and littermate controls of both sexes with age, provides a mechanism to evaluate brain changes in network function which align closely with previous clinical stages of AD. Moreover, utilizing open-source clinical tools from the Brain Connectivity Toolbox (BCT), we demonstrated that brain networks reorganize with AD progression at multiple levels, and these changes are consistent with previous reports in human AD studies.

FUTURE DIRECTIONS: The open-source framework developed in the current work, provides valuable tools for brain metabolic covariance modeling which can be used in both preclinical and clinical settings, and enables more direct translation of preclinical imaging studies to those in the clinic. When matched with an appropriate animal model, genetics, and/or treatments, this study will enable assessment of *in vivo* target engagement, translational pharmacodynamics, and insight into potential treatments of AD.

INTRODUCTION

Alzheimer's disease (AD) represents the leading cause of dementia worldwide, and currently there are few approved therapies to slow, prevent or reverse the disease process [1, 2]. The number of people affected by AD in the US is expected to reach 14 million by 2050, which translates into a financial burden that will exceed 9 trillion dollars worldwide [3]. The molecular characteristics of AD are extracellular β-amyloid (Aβ) plaque formation, and accumulation of hyperphosphorylated tau which form neurofibrillary tangles, and lead to inflammation, synaptic impairment, and cognitive decline [1, 2]. Coupled to these changes, anatomical investigations with magnetic resonance imaging (MRI) have revealed atrophy as a consequence of AD neuropathology [4]. Additionally, molecular imaging with positron emission tomography (PET) of amyloid, tau, and glycolytic metabolism [5], have demonstrated a clinical utility for neuroimaging in predictive/clinical diagnosis and care for AD and related dementias. Several prior studies, in both nonhuman and human samples, have shown altered regional metabolic demands in AD, as measured with ^{18}F-2-fluorodeoxyglucose (^{18}F-FDG) PET [6-9], where AD was associated with regional hypometabolism in the brain. By contrast, in early probable AD stages (referred to as asymptomatic preclinical or at at-risk stages), regional hypermetabolism has been shown [10, 11]. Furthermore, recent work suggests that AD progression clinically is linked to alterations in metabolic activity of brain networks (default mode network and AD-related pattern) measured by ^{18}F-FDG PET [12].

In addition to measures of regional alterations with AD, inter-regional relationships have be investigated though applications of graph theory and network neuroscience (for review, see Bassett and Sporns [13]). Specifically, with reference to ^{18}F-FDG PET, these relationships are often referred to as metabolic connectivity or metabolic covariance networks [14] and can be quantified as inter-subject covariance networks (cross-correlation of regional values across a homogenous sample or group) [15], which have been observed in healthy older adults, and is in-part related to functional connectivity networks [16]. Alternations in metabolic covariance have also been reported in multiple degenerative diseases [15, 17-20]. Among them, the AD group was shown to have altered metabolic connectivity [14], including increased entropy, connection strength, and clustering coefficient [15].

However, in preclinical rodent models of AD, there is a lack of consensus among ^{18}F-FDG PET studies (for review see [21]). The 5XFAD mouse model, which expresses five mutations of human familial AD genes [22], has been shown to have both increased [23] and decreased ^{18}F-FDG-measured glucose metabolism [8, 24]. Variability in outcomes is likely due to methodological differences, notably whether the animals were anesthetized, fasted, and how tracer uptake was handled. Regional analysis has typically utilized standardized uptake values (SUV), which assume that the total volume of distribution of the tracer is related to the body mass and seek to normalize the regional distribution by this factor.

Alternatively, SUV ratios (SUVR) have also been used, which represent the uptake as a ratio of the region
of interest to a reference region (i.e., cerebellum or corpus callosum), thus minimizing dose and noise
effects. In addition, outcome variability may also be due to underlying genetics and pathological
fluctuations in cerebral metabolism in AD across measurements. Collectively these studies reinforce the
importance of *in vivo* imaging of AD neuropathology and suggest that analysis of glycolytic metabolism
via interregional covariance may provide valuable insights into AD progression. In this study, we explored
whether a metabolic covariance structure in ^{18}F-FDG derived networks from mice differed in 5XFAD
compared to wild-type (WT) animals with sex and age. We hypothesized that 5XFAD mice cohorts will
display characteristics indicative of neurodegeneration and disrupted glucose update/utilization in their
networks compared to their WT counterparts.

METHODS AND MATERIALS

5XFAD Transgenic Mouse Model

5XFAD overexpress five familial Alzheimer's Disease (FAD) mutations: the APP (695) transgene includes
the Swedish (K670N, M671L), Florida (I716V), and London (V717I) mutations, and the PSEN1 transgene
accounts for the M146L and L286V FAD mutations. The 5XFAD line was made congenic on the C57BL/6J
background in 2011 at Jackson Laboratories to minimize concerns related to allele segregation and the
high variability of the original hybrid background. 5XFAD mice exhibit cerebral amyloid deposition, gliosis,
and progressive neurodegeneration accompanied by cognitive and motor deficiencies, recapitulating
many of the features of human AD. However, studies have shown that neurofibrillary tangles (NFTs) are
not typically present in the 5XFAD model [25], indicating a key distinction between AD pathology in human
disease and the 5XFAD model.

Animal Housing

Male hemizygous 5XFAD mice (MMRRC stock #: 34848) were crossed with female C57BL6/J mice (JAX
stock #: 000664) to maintain the 5XFAD and non-transgenic WT colonies at Indiana University. Up to
five mice were housed per cage with Aspen SaniChip bedding and ad libitum LabDietR 5K52/5K67 (6%
fat) feed. The colony room was kept on a 12:12 schedule with the lights on from 7:00 AM to 7:00 PM
daily. Transgenic and WT mice were initially ear punched for identification; following genotyping, mice
were identified with p-chip (PharmaSeq) microchips placed at the base of the tail. Both male and female
littermate mice aged 4, 6, and 12 months old were used for this study. These ages reflect early disease
state (4 months), moderate disease state (6 months), and late disease state (12 months). In all cases,
non-transgenic littermates were used as WT controls. All studies were approved by the Institutional
Animal Use and Care Committees (IACUC) at Indiana University School of Medicine.

Magnetic Resonance Imaging (MRI)

High-contrast gray matter images were acquired at least 2 days prior to PET imaging, where mice were anesthetized (induced with 5% isoflurane in medical oxygen, maintained with 1–3% isoflurane). High-resolution T2- weighted (T2W) MRI images were acquired using a 3T Siemens Prisma MRI scanner (Singo, v7.0), outfitted with a 4-channel head coil, anesthesia, and bed system (RAPID MR, Columbus, OH, United States). SPACE3D images were acquired with the following parameters: TA: 5.5 min; TR: 2080 ms; TE: 162 ms; ETL: 57; FS: On; Average: 2; Excitation Flip Angle: 150; Norm Filter: On; Restore Magnetization: On; Slice Thickness 0.2 mm; Matrix: 171 x 192; and FOV: 35 x 35 mm, yielding 0.18 x 18 x 0.2 mm resolution images.

^{18}F-FDG Positron Emission Tomography (PET) Image Acquisition

Prior to tracer administration, mice were fasted for a minimum of 12 hours. Mice were injected intraperitoneally (IP) with 3.7 to 9.25 MBq (100 to 250 µCi) of ^{18}F-FDG, with the final volume not exceeding 10% of the animal's weight. After injection, mice were placed in their home cage for 45 minutes to allow for tracer uptake [22]. The mice were then anesthetized with 5% isoflurane gas, positioned on the imaging bed, and scanned on the IndyPET3 scanner [26]. During acquisition, anesthetic plane was maintained with 1-3% isoflurane. Post listmode data collection, PET images were calibrated, decay and scatter-corrected, and reconstructed into a single-static image volume with a 60 mm field of view using filtered-back-projection [27], with an effective resolution of 1.1 x 1.1 x 1.2 mm (1.45 mm^3). Images were converted from NetCDF to an Analyze 12-compatible format prior to analysis.

Image Preprocessing

PET and MRI images were co-registered to stereotactic mouse brain coordinates [28] using a rigid-body mutual information-based normalized entropy algorithm with 9 degrees of freedom implemented in Analyze 12 (AnalzeDirect, Stilwell, KS, United States). After registration, 56 bilateral regions were extracted, SUVR values (ratio to the cerebellum) computed, and left and right regions were averaged:

$$SUVR(s, R, g, a) = \frac{R(s,g,a)}{C(s,g,a)} \tag{1}$$

where the standardized update value ratio (SUVR) for a given animal (*s*), region (*R*), genotype (*g*), and age (*a*), is the ratio of the region of interest activity *R(s,g,a)* and cerebellar reference region activity *C(s,g,a)* in Bq/ml. To minimize the likelihood of partial volume effects, region volumes were selected where the smallest region (i.e. fornix = 178 mm^3) exceeded the effective scanner sample volume by ≥ 123 fold. At the limit, using a partial volume factor of 5 voxels, the smallest resolvable effective volume would be 7.25 mm^3, and therefore is well within the smallest region volume used in the current study.

Covariance Network Analysis

Network analysis was computed in Matlab (MathWorks, version 2021b; Natick, MA) with the use of the
Brain Connectivity Toolbox (BCT) [29], generalized Louvain modularity [30], and hierarchical consensus
clustering [31]. Analysis code is publicly available in the CovNet package
(https://github.com/echumin/CovNet).

Network Estimation and Thresholding

Covariance networks were computed for 3 age groups (4, 6, and 12 months) of WT (males: n=12, 11, 9;
females n=12, 11, 10) and 5XFAD mice (males: n=11, 10, 9; females: n=12, 12, 10), using Pearson
correlation of regional *z*-scored SUVR values across animals within group. The resultant covariance
network for each group is then a region-by-region (27 x 27 region) adjacency matrix that indicates degree
of similarity of ^{18}F-FDG quantified metabolic coupling among all region pairs. Three network variants were
generated: 1) weighted unthresholded; 2) weighted thresholded at $p < 0.05$ correlation significance; and
3) weighed thresholded at $p < 0.01$. Edge-level correlation significance was assessed with a random shift
null model, where SUVR values were permuted independently for each region (i.e. shuffling animals
within group), destroying the covariance structure with 10,000 permutations. The distribution of 10,000
null covariance networks was then used to estimate permutation p-values at each edge as the fraction of
times the empirical correlation exceed the null in magnitude (positive and negative correlations were
handled separately). Modularity maximization was performed on unthresholded networks as they contain
the most information, while both unthresholded and thresholded networks were used to assess network
properties. Thresholds below $p < 0.01$ were not investigated as they produced fractured networks (where
a node or a group of nodes are disconnected from the rest of the network) in more than half of the groups.

Global and Nodal Network Measures

The following network measures were computed on thresholded networks using BCT: network density –
number of connections, node degree – number of connections for each region, positive and negative
nodal strengths – sum of the positive or negative covariance values for each region, clustering coefficient
– number of fully connected triangles around a node taking into account the weight and sign of the
connections (coefficient type 3 in the BCT clustering_coef_wu_sign function) [32]. Two variants of hub
regions were also identified as the top quartile (7 regions) in network strength (strength-based)
(cumulative strength computed as the sum of the absolute values) or degree (degree-based). Strength-
based hubs were estimated from unthresholded and thresholded networks, while degree-based hubs
were estimated from thresholded networks only.

Multiresolution Consensus Clustering

Community detection, also referred to as modularity maximization, is the process of identifying a partition
of nodes in a network into groups or communities, such that within community connectivity is greater than
between community. However, this raises an issue of scale, asking what is the optimal number of
communities in a network? While there is no correct answer to this question, the Multiresolution
Consensus Clustering (MRCC) [31] approach addresses this by identifying communities across spatial
scales, and then quantitatively identifying a consensus partition from the set. Here MRCC was applied to
weighted unthresholded networks, generating a set of 10,000 initial partitions. From this set of partitions,
MRCC then computes a co-assignment matrix (i.e. probability that any node pair is in the same
community), a dendrogram of partitions across spatial scale, and a consensus partition given an alpha
threshold ($\alpha = 0.05$). The derived consensus partitions were then qualitatively compared and used to
investigate group differences in mean module/community SUVR values.

Statistical Analysis

Edge weight distributions of networks as well as distributions of nodal measures (i.e. degree, strength,
and clustering coefficient) were compared between groups via 2-sample Kolmogorov Smirnov (KS) tests.
Pairwise edge-level differences in group covariance networks were assessed with permutation *t*-tests
(10,000 group label permutations on regional SUVR values, recomputing a null covariance network at
each permutation). Multiple comparisons correction for number of edges (i.e. connections) was done with
a false discovery rate (FDR) adjusted at *q*<0.05. Module average SUVR values were extracted from all
groups using a single groups partition as reference (https://github.com/echumin/CovNet/releases/tag/fdg-
pet-mouse), so that the same regions are being averaged for all groups. An n-way analysis of variance
(Matlab) with, age, sex, and genotype as factors, was used to test for main effects and two-way
interactions. In the presence of significant effects, post hoc multiple comparisons were assessed with
Tukey-Kramer.

RESULTS

Characterization of Group Covariance

Metabolic covariance matrices and distributions of edge weights (i.e. Pearson correlations) are shown in
Figure 1. WT covariance matrices were qualitatively more structured compared to 5XFAD, notably in
males. Pairwise KS tests comparing male versus female networks within genotype showed that only the
WT 6-month network-derived edge weight distributions were significantly different (Figure 1B, KS statistic
0.14, *p* < 0.005). Thresholded covariance networks for *p's* < 0.05 and 0.01 are shown in Figures S1 and
S2, respectively. Between WT and 5XFAD, distributions of edges weights were not different with

Figure 1. Metabolic (^{18}F-FDG PET) covariance matrices for (A-C) wild-type (WT) and (D-F) 5XFAD groups. Histograms show the correlation coefficient distributions from male (lower triangle of matrix) and female (upper triangle of matrix) covariance matrices at 4 months (A,D), 6 months (B,E), and 12 months (C,F) old. Covariance was computed as Pearson correlation of *z*-scored regional standardized uptake value ratios across animals within each group. Full names for row/column region labels can be found in Table S1. For visualizations of thresholded networks see Figure S1 and S2 for $p < 0.05$ and $p < 0.01$ correlation significance, respectively.

exception of females at 12 months (Figure 2F, KS statistic 0.1, $p < 0.05$). Edgewise group comparisons
were carried out with permutation testing, with edges below $p < 0.05$ shown in Figure 2. No individual
edges survived FDR correction. In male mice at 4 months, at $p < 0.05$ uncorrected significance, 4 regions
stand out as having altered coupling to a large portion of the other regions in the network: the ventral,
medial, and lateral orbitofrontal cortices, and the fornix (Figure 2A). Differences in females at 4 months
identified the agranular insular and dysgranular insular cortices with the most differences to the rest of
the network (Figure 2D). At 6 months of age for both sexes, some edge-wise differences were identified,
but no regions showed differences to a notable portion of the rest of the network (Figure 2B,E). Finally,
at 12 months, multiple regions showed differences with ~20% of the network (i.e. secondary

somatosensory, retrosplenial dysgranular, perirhinal and perilimbic cortices, hippocampus, fornix, auditory and frontal association cortices; Figure 2C), while in females only the ventral orbital cortex stood out (Figure 2F).

Figure 2. Covariance network comparisons across genotype. Histograms are distributions of network edge weights statistically compared with a Kolmogorov-Smirnov test at $p < 0.05$ threshold. Only in Females at 12 months (F) were the distributions significantly different. Individual edges were tested for group differences with permutation testing (10,000 permutations), with matrices showing uncorrected significance at $p < 0.05$. Multiple comparisons were assessed with FDR, with no adjusted significant edges identified.

Examining the global network properties, network densities (i.e. number of connections) showed a decrease with increase age at both p-value thresholds in WT male mice, with 5XFAD male mice showing an already lower density (relative to WT) at 4 months, was similar at 6 months and drastically lower at 12 months (Figure 3A). Female mice showed an inverted u-shape pattern across age that was similar in

both WT and 5XFAD groups, with one distinction that the 5XFAD female mice network had a higher

density relative to WT at 12 months (Figure 3A). Nodal network properties followed a similar pattern seen

with network density, which is expected given the strong impact of network density on other network

metrics [29]. Pairwise comparisons across genotype identified differences in distributions of nodal degree

(i.e. number of connections; Figure 3B) and positive and negative nodal strength (i.e. sum of positive and

negative edge weights, or correlation coefficients, respectively; Figure 3C,D) in both sexes and multiple

age groups. Differences in clustering coefficient (i.e. measure of network segregation, or how many of

the nodes' connected neighbors are connected to each other) between WT and 5XFAD were only seen

in female groups (Figure 3E). At a more restrictive network threshold of $p < 0.01$, a similar pattern of

differences was observed (Figure S3).

Figure 3. Properties of thresholded covariance networks for wild-type (WT) and 5XFAD groups at 4, 6, and 12 months old. **(A)** Network densities ($p < 0.05$ and 0.01). **(B)** Degree, **(C)** positive and **(D)** negative strength, and **(E)** clustering coefficient nodal distributions of $p < 0.05$ thresholded covariance networks. Degree, strength, and clustering coefficient for $p < 0.01$ thresholded networks were lower in magnitude (as expected) but overall similar (Figure S3). *Denotes $p < 0.05$ 2-sample Kolmogorov-Smirnov test significance.

244   *Hubs of Metabolic Covariance*

245   While there was some overlap in hub regions overall, uniquely identified hubs showed a divergence by

246   genotype (i.e. WT and 5XFAD) in this study. When hubs were defined based on strength (i.e. sum of

247   weights, Figure 4), the difference between WT and 5XFAD networks tended to increase proportionate to

248   age. With respect to sex, males tended to express a greater magnitude of alterations in strength hubs

Figure 4. Covariance network strength hubs. Of the 27 nodes in the covariance networks, regions with the top 25% (7 regions) nodal strength were labeled as hubs for each group. Strength hubs are color coded based on whether they were identified in WT (blue), 5XFAD (red), or both (green) groups for unthresholded (A) and $p < 0.05$ and 0.01 thensholded (B-C) networks. Spatial location of strength hubs from unthresholded networks for WT (D) and 5XFAD (E) groups is shown on a magnetic resonance image template for female (red) and male (blue) groups at youngest (top) and oldest (bottom) investigated age. Left/Right hemisphere separation by sex is for visualization only. Images for all ages as well as all network threshold strength hubs are shown in Figure S4. Region labels are in Table S1.

compared to females. Females at 6 months, as with above discussed metrics, were similar between WT
and 5XFAD, which was not the case for either 4- or 12-month female groups. Alternatively, defining hubs
based on highest degree (i.e. number of connections) implicated a similar set of regions (Figure 5).

Community/Modularity Structure of Metabolic Covariance

Leveraging a data driven approach to derive a consensus community structure from networks that does
not require a selection of scale [31], we identified a consensus partition for each unthresholded group
covariance network (Figure 6A). Partitions of WT networks for both sexes revealed a coarse consensus
structure comprised largely of 2-3 communities. The exception was the 12-month female group, which
had a finer scale consensus community structure of 7 communities. Relative to WT, the number of
communities was greater in 5XFAD groups (with exception of 4-month male and 6-month female 5XFAD
groups). Number of communities can be interpreted as an indicator of coherence among regions in the
network, therefore, the observed higher community counts in 5XFAD groups demonstrate a disordered
underlying metabolic covariance structure of those networks. Quantitative comparison of partition

Figure 5. Covariance network degree hubs. Of the 27 nodes in the covariance networks, regions with the top 25% (7 regions) nodal degree were labeled as hubs for each group. Degree hubs are color coded based on whether they were identified in WT (blue), 5XFAD (red), or both (green) groups for $p < 0.05$ (A) and 0.01 thensholded networks. Spatial location of degree hubs from $p < 0.05$ networks for WT (C) and 5XFAD (D) groups are shown on a magnetic resonance image template for female (red) and male (blue) groups at youngest (top) and oldest (bottom) investigated age. Left/Right hemisphere separation by sex is for visualization purposes only. Images for 6-month age group degree hubs are shown in Figure S5. Region labels are in Table S1.

similarity among groups with adjusted mutual information (AMI) [33] showed diversity among consensus partitions, with no clear distinctions of age, sex, or genotype (Figure 6B). Co-classification (i.e. per node pair, the fractions of instances in which they were assigned to the same community) of consensus partitions within genotype revealed that WT groups had greater agreement for several regions, as seen in the Figure 6C co-classification matrix (left) and regional averages (right). Using the 4-month male WT partition as reference, mean SUVR values for the two modules were extracted and compared in a 3-way ANOVA (genotype, sex, and age as factors). For module 1 (Figure 6D), there was a main effect of age (F=9.9, $p < 0.0005$) as well as an age*sex interaction (F=4.68, $p < 0.05$). Post hoc tests revealed that 4- and 12-month groups were different from 6-month groups (Tukey-Kramer adjusted $p < 0.05$). No main effects or interactions were identified for module 2 (Figure 6E).

DISCUSSION

We used a network connectivity analysis approach to understand group alterations in metabolic networks between and early-onset AD mouse model (5XFAD) and wild-type control groups (WT) at 4, 6, and 12 months in both sexes. Our networks estimates from ^{18}F-FDG SUVR WT groups displayed interregional structure that was altered in 5XFAD groups. While having similar distributions of edge weights among

Figure 6. (A) Consensus modular structure for all groups (columns) with color indicating community assignment for each region (rows). (B) Adjusted mutual information matrix, quantifying the similarity of partitions among groups on a scale of zero (completely different) to one (identical). (C) Regional co-classification matrices computed from partitions of groups within genotype. WT data are in lower triangle and 5XFAD data are in the upper triangle. Average co-classification for each region within group is shown to the right of the matrix. (D-E) Using the 4-month male WT partition as reference, mean module SUVR values were extracted and are shown for (D) module 1 (corresponding to regions in blue in A for the 4-month male WT partition) and (E) module 2 (orange in the reference partition). Full names for row region labels in A can be found in Table S1.

the networks (Figure 1), multiple regions were found to differ in their covariance across genotype (Figure 2). Global and nodal network properties (i.e. density, degree, strength, clustering) showed a linear decrease with age in male and an inverted u-shape in female groups, with 5XFAD showing reductions in nodal degree and strengths, and differences in clustering of 5XFAD female group networks (Figure 3).

These alterations in network structure indicate that AD pathology is disrupting metabolic coupling, which
is consistent with clinical evidence of glucose alterations in AD [34].

Previous studies have reported both increases [23, 35] as well as decreases [8, 24] in ^{18}F-FDG uptake
of 5XFAD animals over the range from 7-12 months, with differences in younger mice. Given the lack of
consensus, we hypothesized that interregional relationships via covariance networks would better show
AD-related alterations in glucose uptake measured with ^{18}F-FDG PET. First, we found a significant
difference in male vs. female weighted distributions in 4-month WT mice, but not in 5XFAD 4-month
cohorts, where the WT females showed more edges with stronger negative covariance (Figure 1B). This
lack of effect could be explained by the aggressive nature of the 5XFAD transgenic model, which likely
overshadows any sex-dependent developmental differences in glucose metabolism [36]. Second, when
comparing weighted distributions across genotype, we found that between 12-month female WT and
5XFAD group networks, there were a significant difference in edges (both positive and negative) in the
5XFAD network (Figure 2F). These covariance networks are statistical constructs (i.e. correlations) that
capture higher-order relationships beyond regional differences. Therefore, changes in the distributions of
weights of these networks do not reflect hyper- or hypometabolism, rather they capture patterns shared
by animals within a homogenous group. Altered ^{18}F-FDG uptake can be reflective of reduced glucose
utilization by the brain regions. These mechanisms are dependent on membrane transport proteins (i.e.
GLUT1-5), which transport glucose across cellular membranes [34], and therefore it is plausible that
regional expression of these proteins in the 5XFAD model contribute to observed alterations in metabolic
covariance observed.

Global and nodal network properties from graph theory provide valuable insight into the organization and
topology of networks. They can determine if networks are comparable, quantify extent and magnitude of
regional interrelationship, and assess clustering topology [13, 37, 38]. The present characterization of
metabolic covariance in 5XFAD model of AD, we showed that in thresholded networks network properties
decreased with increasing age of group, with exception of clustering coefficient. A recent study also
reported age-related changes in metabolic covariance in young (2 months) versus old (18 months)
Sprague-Dawley rats, reporting some edge, but not path-based global network measure differences [39].
Importantly, path based measures utilized in Xue, Wu [39] were developed for structural connectivity
networks and their interpretations in functional connectivity or metabolic covariance networks are unclear.
Interestingly, the shape of decline observed differed between groups, with networks of male groups
showing a linear decline, while female groups showed and inverted u-shape. These patterns across age
(Figure 3) were present in both WT and 5XFAD; however, male 5XFAD groups showed reductions at the
earliest age of 4 months, while female 5XFAD groups showed increases at the latest time point (12
months). Increasing attention is being given in recent years to sex specific differences in AD vulnerability

and progression, noting faster decline greater pathology in women [40, 41], which is consistent with our
findings.

Identifying nodes that show high connectivity/coupling to the rest of the network [38], known as hubs, can
highlight key regions within networks. For metabolic covariance networks, hubs (here defined on degree
and strength), are regions that showed a similar ^{18}F-FDG SUVR pattern across animals with many other
regions in the brain. There was a moderate degree of overlap among age, sex, and genotype. Notable
nodes involved regions of the dorsal striatum, and entorhinal, parietal, and perirhinal cortices.
Interestingly, the hippocampus reached our defined hub threshold only in the 5XFAD groups (Figure 4),
while primary and secondary motor cortices were metabolic hubs only in WT younger male groups, and
older male 5XFAD as well as female groups (ages 4 and 12 months). The strong covariance of these
regions aligns with previous reports in mouse and rat, which identified them as hubs in resting state
functional MRI data [42, 43].

In addition to identifying potential hubs, we utilized data driven modularity to identify community structure
in the network of each group. Modules are characterized by greater within module connectivity than to
between modules. Identifying the modular structure in a network is therefore an optimization problem;
however, it can yield solutions of varying community number size [44]. Here we employed multiresolution
consensus clustering, which spans a space of module solutions across scale and statistically identifies a
consensus modular partition [31]. For the twelve groups investigated here, modular partitions ranged in
size 2 -7 modules. WT group networks had fewer modules, which indicated a high degree of similarity of
across animals, while 5XFAD groups has a generally greater number of communities. Assessing overall
similarity between all group pairs did not reveal any distinction of age, sex, or genotype. As a follow-up
nodal similarity in community assignment (i.e. co-classification) within genotype showed a pattern within
WT groups that was disrupted in 5XFAD groups (Figure 6C). This difference further highlights the
increased variability in metabolic covariance due to mutations in the 5XFAD model. Examining the
community structure more closely (see Figure 6A), it is apparent that functional connectivity in the 12-
month WT females are stratified based on function, with insular regions in module 1, auditory in module
2, rhinal in module 3, parietal in module 7, and orbitofrontal and limbic regions dispersed between the
modules. The 12-month 5XFAD females, on the other hand, displayed similar all-in functional groupings
in modules, but with more functional groups in each module. Module 1 contained all auditory, insular, and
rhinal regions, module 2 had all basal ganglia and white matter, module 3 had the majority or orbitofrontal
regions, and module 4 contained most of the parietal regions.

These findings extend our understanding of AD progression by modeling interregional relationships of
glycolytic metabolism via ^{18}F-FDG PET in 5XFAD mice; however, there are limitations to consider. Firstly,

this is across sectional investigation with groups spanning age, sex, and genotype. Although the 5XFAD

mice were from the same parental stock, and are therefore genetically identical, there is a possibility that

rearing mice from different mothers, with unique microbiomes, could influence the ^{18}F-FDG PET signals.

Recent work has shown that C56BL6/J mice with identical rearing conditions have distinct gut microbiota,

which has been reported to impact brain immune cell profiles and modulates cognitive and affective

behavior in mice [45], and thus would be reflected in the uptake. To resolve these changes, one could

construct within subject metabolic networks from dynamic ^{18}F-FDG PET studies. Secondly, the use of

transgenic models, such as the 5XFAD, which over-express amyloid precursor protein, are known to

show a strong sexual dimorphism resulting from the transgene expression being linked to the estrogen

sensitive Thy1 promotor [46]. As the next generation of models are released from Model Organism

Development & Evaluation for Late-Onset AD (MODEL-AD; www.model-ad.org), which do not employ

transgenes, many of these issues will be overcome, thus clarifying the true role of sex in AD. Finally,

harmonization of the analysis methods for the primary data is needed. As described above, numerous

analytical methods have been used in the literature to standardize uptake of ^{18}F-FDG in both preclinical

and clinical studies; however, each has significant limitations and none can be used universally across

species. In the case of SUVs, which make up the source information used for z-score transformed

correlations, there is a possibility that the transformations themselves may artificially bias the results

based on body weight differences alone. In the current study, we employed SUVR, using the cerebellum

as a reference region, which is used in the AD Neuroimaging Initiative [47]; however, since the cerebellum

is not a true "null" region, there is a chance that this normalization could introduce bias. Our results align

with previous clinical findings [15], providing some level of assurance that the current approach is not

tangibly biased. Future studies could leverage the covariance framework to investigate the role of

vasculature in conjunction with metabolism, as prior studies have found a neurovascular uncoupling

effect that consistently follows a pattern in AD as a function of disease progression and aging.[48, 49].

Additionally, future studies could employ multi-omic/-modal analyses that generate and combine network

data from PET (amyloid, tau, metabolic) and MRI (structural and functional) to obtain a more detailed

understanding of the pathophysiology of AD.

CONCLUSIONS

To our knowledge, this is the first comprehensive evaluation of metabolic covariance structure in the

5XFAD model of AD. The 5XFAD model mice show age related changes in interregional glucose uptake

relationships that are altered relative to WT mice. Moreover, analysis of these data revealed that

community structure of covariance networks was different across age and sex, with a disruption of

interregional metabolic coupling in 5XFAD model of AD.

REFERENCES

[1] Karch Celeste M, Cruchaga C, Goate Alison M. Alzheimer's Disease Genetics: From the Bench to
the Clinic. Neuron. 2014;83:11-26.

[2] Citron M. Alzheimer's disease: strategies for disease modification. Nature Reviews Drug Discovery.
2010;9:387-98.

[3] Jia J, Wei C, Chen S, Li F, Tang Y, Qin W, et al. The cost of Alzheimer's disease in China and re-
estimation of costs worldwide. Alzheimer's & Dementia. 2018;14:483-91.

[4] Vemuri P, Jack CR. Role of structural MRI in Alzheimer's disease. Alzheimer's Research & Therapy.
2010;2:23.

[5] Nordberg A, Rinne JO, Kadir A, Långström B. The use of PET in Alzheimer disease. Nature
Reviews Neurology. 2010;6:78-87.

[6] Friedland RP, Budinger TF, Ganz E, Yano Y, Mathis CA, Koss B, et al. Regional Cerebral Metabolic
Alterations in Dementia of the Alzheimer Type: Positron Emission Tomography with [18: 18:]
Fluorodeoxyglucose. Journal of Computer Assisted Tomography. 1983;7.

[7] Cohen AD, Klunk WE. Early detection of Alzheimer's disease using PiB and FDG PET.
Neurobiology of Disease. 2014;72:117-22.

[8] Macdonald IR, DeBay DR, Reid GA, O'Leary TP, Jollymore CT, Mawko G, et al. Early Detection of
Cerebral Glucose Uptake Changes in the 5XFAD Mouse. Current Alzheimer Research.
2014;11:450-60.

[9] Latimer CS, Shively CA, Keene CD, Jorgensen MJ, Andrews RN, Register TC, et al. A nonhuman
primate model of early Alzheimer's disease pathologic change: Implications for disease
pathogenesis. Alzheimer's & Dementia. 2019;15:93-105.

[10] Johnson SC, Christian BT, Okonkwo OC, Oh JM, Harding S, Xu G, et al. Amyloid burden and
neural function in people at risk for Alzheimer's Disease. Neurobiology of Aging. 2014;35:576-84.

[11] Yi D, Lee DY, Sohn BK, Choe YM, Seo EH, Byun MS, et al. Beta-Amyloid Associated Differential
Effects of APOE ε4 on Brain Metabolism in Cognitively Normal Elderly. The American Journal of
Geriatric Psychiatry. 2014;22:961-70.

[12] Perovnik M, Tang CC, Namías M, Eidelberg D, Alzheimer's Disease Neuroimaging I. Longitudinal
changes in metabolic network activity in early Alzheimer's disease. Alzheimer's & Dementia.
2023;n/a.

[13] Bassett DS, Sporns O. Network neuroscience. Nature Neuroscience. 2017;20:353.

[14] Sala A, Lizarraga A, Caminiti SP, Calhoun VD, Eickhoff SB, Habeck C, et al. Brain connectomics:
time for a molecular imaging perspective? Trends Cogn Sci. 2023;27:353-66.

[15] Veronese M, Moro L, Arcolin M, Dipasquale O, Rizzo G, Expert P, et al. Covariance statistics and
network analysis of brain PET imaging studies. Scientific Reports. 2019;9:2496.

[16] Di X, Biswal, Alzheimer's Disease Neuroimaging Initiative BB. Metabolic Brain Covariant Networks
as Revealed by FDG-PET with Reference to Resting-State fMRI Networks. Brain Connectivity.
2012;2:275-83.

[17] Ma Y, Huang C, Dyke JP, Pan H, Alsop D, Feigin A, et al. Parkinson's Disease Spatial Covariance
Pattern: Noninvasive Quantification with Perfusion MRI. Journal of Cerebral Blood Flow &
Metabolism. 2010;30:505-9.

[18] Feigin A, Leenders KL, Moeller JR, Missimer J, Kuenig G, Spetsieris P, et al. Metabolic Network
Abnormalities in Early Huntington's Disease: An [18F]FDG PET Study. Journal of
Nuclear Medicine. 2001;42:1591-5.

[19] Titov D, Diehl-Schmid J, Shi K, Perneczky R, Zou N, Grimmer T, et al. Metabolic connectivity for
differential diagnosis of dementing disorders. Journal of Cerebral Blood Flow & Metabolism.
2015;37:252-62.

[20] Perneczky R, Drzezga A, Diehl-Schmid J, Li Y, Kurz A. Gender differences in brain reserve.
Journal of Neurology. 2007;254:1395-400.

[21] Bouter C, Bouter Y. 18F-FDG-PET in Mouse Models of Alzheimer's Disease. Frontiers in Medicine.
2019;6.

[22] Oblak AL, Lin PB, Kotredes KP, Pandey RS, Garceau D, Williams HM, et al. Comprehensive
Evaluation of the 5XFAD Mouse Model for Preclinical Testing Applications: A MODEL-AD Study.
Frontiers in Aging Neuroscience. 2021;13.

[23] Rojas S, Herance JR, Gispert JD, Abad S, Torrent É, Jiménez X, et al. In vivo evaluation of
amyloid deposition and brain glucose metabolism of 5XFAD mice using positron emission
tomography. Neurobiology of Aging. 2013;34:1790-8.

[24] Franke TN, Irwin C, Bayer TA, Brenner W, Beindorff N, Bouter C, et al. In vivo Imaging With 18F-
FDG- and 18F-Florbetaben-PET/MRI Detects Pathological Changes in the Brain of the Commonly
Used 5XFAD Mouse Model of Alzheimer's Disease. Frontiers in Medicine. 2020;7.

[25] Oakley H, Cole SL, Logan S, Maus E, Shao P, Craft J, et al. Intraneuronal β-Amyloid Aggregates,
Neurodegeneration, and Neuron Loss in Transgenic Mice with Five Familial Alzheimer's Disease
Mutations: Potential Factors in Amyloid Plaque Formation. The Journal of Neuroscience.
2006;26:10129-40.

[26] Rouzes A, Berthoin K, Xuereb F, Djabarouti S, Pellegrin I, Pellegrin JL, et al. Simultaneous
determination of the antiretroviral agents: amprenavir, lopinavir, ritonavir, saquinavir and efavirenz

in human peripheral blood mononuclear cells by high-performance liquid chromatography–mass
spectrometry. Journal of Chromatography B. 2004;813:209-16.

[27] Soon VC, Miller MA, Hutchins GD. A non-iterative method for emission tomographic image
reconstruction with resolution recovery. 2007 IEEE Nuclear Science Symposium Conference
Record2007. p. 3468-73.

[28] Franklin KBJ, Paxinos G. Paxinos and Franklin's The mouse brain in stereotaxic coordinates.
Fourth edition ed. Amsterdam: Academic Press, an imprint of Elsevier; 2013.

[29] Rubinov M, Sporns O. Complex network measures of brain connectivity: Uses and interpretations.
NeuroImage. 2010;52:1059-69.

[30] Mucha PJ, Richardson T, Macon K, Porter MA, Onnela J-P. Community Structure in Time-
Dependent, Multiscale, and Multiplex Networks. Science. 2010;328:876.

[31] Jeub LGS, Sporns O, Fortunato S. Multiresolution Consensus Clustering in Networks. Scientific
Reports. 2018;8:3259.

[32] Costantini G, Perugini M. Generalization of Clustering Coefficients to Signed Correlation Networks.
PLOS ONE. 2014;9:e88669.

[33] Nguyen Xuan Vinh, Julien Epps, Bailey J. Information Theoretic Measures for Clusterings
Comparison: Variants, Properties, Normalization and Correction for Chance. Journal of Machine
Learning Research. 2010;11:2837-54.

[34] Szablewski L. Brain Glucose Transporters: Role in Pathogenesis and Potential Targets for the
Treatment of Alzheimer's Disease. International Journal of Molecular Sciences2021.

[35] Choi H, Choi Y, Lee EJ, Kim H, Lee Y, Kwon S, et al. Hippocampal glucose uptake as a surrogate
of metabolic change of microglia in Alzheimer's disease. Journal of Neuroinflammation.
2021;18:190.

[36] Bouter C, Irwin C, Franke TN, Beindorff N, Bouter Y. Quantitative Brain Positron Emission
Tomography in Female 5XFAD Alzheimer Mice: Pathological Features and Sex-Specific
Alterations. Frontiers in Medicine. 2021;8.

[37] Sporns O, Betzel RF. Modular Brain Networks. Annu Rev Psychol. 2016;67:613-40.

[38] van den Heuvel MP, Sporns O. Network hubs in the human brain. Trends in Cognitive Sciences.
2013;17:683-96.

[39] Xue X, Wu J-J, Huo B-B, Xing X-X, Ma J, Li Y-L, et al. Age-related alterations of brain metabolic
network based on [18F]FDG-PET of rats. Aging. 2022;14:923-42.

[40] Ferretti MT, Iulita MF, Cavedo E, Chiesa PA, Schumacher Dimech A, Santuccione Chadha A, et al.
Sex differences in Alzheimer disease — the gateway to precision medicine. Nature Reviews
Neurology. 2018;14:457-69.

[41] Guo L, Zhong MB, Zhang L, Zhang B, Cai D. Sex Differences in Alzheimer's Disease: Insights
From the Multiomics Landscape. Biological Psychiatry. 2022;91:61-71.

[42] Mechling AE, Hübner NS, Lee H-L, Hennig J, von Elverfeldt D, Harsan L-A. Fine-grained mapping
of mouse brain functional connectivity with resting-state fMRI. NeuroImage. 2014;96:203-15.

[43] D'Souza DV, Jonckers E, Bruns A, Künnecke B, von Kienlin M, Van der Linden A, et al. Preserved
Modular Network Organization in the Sedated Rat Brain. PLOS ONE. 2014;9:e106156.

[44] Fortunato S, Hric D. Community detection in networks: A user guide. Physics Reports. 2016;659:1-
44.

[45] Abdel Aziz N, Berkiks I, Mosala P, Brombacher TM, Brombacher F. Environmental and microbial
factors influence affective and cognitive behavior in C57BL/6 sub-strains. Frontiers in Immunology.
2023;14.

[46] Moechars D, Lorent K, De Strooper B, Dewachter I, Van Leuven F. Expression in brain of amyloid
precursor protein mutated in the alpha-secretase site causes disturbed behavior, neuronal
degeneration and premature death in transgenic mice. The EMBO Journal. 1996;15:1265-74.

[47] Jagust WJ, Landau SM, Koeppe RA, Reiman EM, Chen K, Mathis CA, et al. The Alzheimer's
Disease Neuroimaging Initiative 2 PET Core: 2015. Alzheimer's & Dementia. 2015;11:757-71.

[48] Tarantini S, Tran CHT, Gordon GR, Ungvari Z, Csiszar A. Impaired neurovascular coupling in
aging and Alzheimer's disease: Contribution of astrocyte dysfunction and endothelial impairment to
cognitive decline. Experimental Gerontology. 2017;94:52-8.

[49] Leuzy A, Rodriguez-Vieitez E, Saint-Aubert L, Chiotis K, Almkvist O, Savitcheva I, et al.
Longitudinal uncoupling of cerebral perfusion, glucose metabolism, and tau deposition in
Alzheimer's disease. Alzheimer's & Dementia. 2018;14:652-63.

DATA AVAILABILITY STATEMENT

The contributions presented in the study are publicly available. The imaging data are available via the AD Knowledge Portal: https://adknowledgeportal.org (permission was obtained for this material through a Creative Commons CC-BY license). The data, analyses, and tools are shared early in the research cycle without a publication embargo on secondary use. Data are available for general research use according to the following requirements for data access and data attribution (https://adknowledgeportal.org/DataAccess/Instructions).

AUTHOR CONTRIBUTIONS

EJC, CB, RS, SCP, AAB, MV, and PRT contributed to conception and design of the study. SCP, AAB, RS and PRT performed studies and initial data analysis. EJC, RS, and PRT developed and tested the analysis software. EJC, CB, and PRT wrote the first draft of the manuscript. EJC, CB performed the statistical analysis. EJC, CB, and PRT wrote sections of the manuscript. All authors contributed to manuscript revision, read, and approved the submitted version.

CONFLICTS OF INTEREST

All authors declare that they have no conflicts of interest to disclose.

FUNDING

EJC - NIA T32 AG071444

PRT - NIA U54 AG054345

MV – NC for HPC CN00000013 CN1; ING PNC0000002_DARE; and WTDA 215747/Z/19/Z

ACKNOWLEDGEMENTS

The authors would like to acknowledge the NIH/NIA and MODEL-AD consortium for making the data available through Open Science principles. The data for this study were funded through grants NIA T32AG071444 and U54AG054345. MV is supported by Italian National Center for HPC, BIG DATA AND QUANTUM COMPUTING (Project no. CN00000013 CN1), the Italian National Grant DIGITAL LIFELONG PREVENTION (Project no PNC0000002_DARE), and by Wellcome Trust Digital Award (no. 215747/Z/19/Z).

KEYWORDS

Alzheimer's disease, preclinical models, metabolic covariance networks, connectomics