3D osteocyte lacunar morphometry of human bone biopsies with high resolution

microCT: from monoclonal gammopathy to newly diagnosed multiple myeloma

Inés Moreno-Jiménez[1*], Sharen Heinig[1], Unai Heras[2], Daniela Simone Maichl[3], Susanne

Strifler[3], Ellen Leich-Zbat[3,4], Stéphane Blouin[5], Peter Fratzl[1], Nadja Fratzl-Zelman[5],

Franziska Jundt[3,6*#], Amaia Cipitria[1,2,7*#]

[1] Max Planck Institute of Colloids and Interfaces, Department of Biomaterials, 14476

Potsdam, Germany

[2] Group of Bioengineering in Regeneration and Cancer, Biodonostia Health Research

Institute, 20014 San Sebastian, Spain.

[3] Department of Internal Medicine II, University Hospital Würzburg, 97080 Würzburg,

Germany

[4] Institute of Pathology, University of Würzburg, 97080 Würzburg, Germany

[5] Ludwig Boltzmann Institute of Osteology at the Hanusch Hospital of OEGK and AUVA

Trauma Centre Meidling, Vienna, Austria.

[6] Comprehensive Cancer Center Mainfranken, 97080 Würzburg, Germany

[7] IKERBASQUE, Basque Foundation for Science, 48009 Bilbao, Spain.

[(*)] Correspondence to: ines.moreno@mpikg.mpg.de; Jundt_f@ukw.de;

amaia.cipitria@mpikg.mpg.de; amaia.cipitria@biodonostia.org

[(#)] These authors contributed equally to this work

Abstract

Osteocytes are bone-embedded cells connected via canaliculi and they regulate the bone

resorption/formation balance. Osteocyte function is altered in skeletal disorders including

cancer. Multiple myeloma (MM) is a hematological malignancy, whereby plasma cells

disrupt the bone homeostasis and induce excessive resorption of the mineralized extracellular

matrix (ECM), as evidenced by clinical computed tomography (CT). However, morphometric

analyses of the mineralized ECM and bone microporosity are not yet performed in patients

with MM, nor in the precursor conditions of monoclonal gammopathy of undetermined

significance (MGUS) and smoldering MM (SMM). Here, we characterize changes in 3D

osteocyte lacunar morphology in bone biopsy samples obtained from patients with MGUS,

SMM and newly diagnosed MM, using high resolution microCT. In the small lacunae 20-900

μm^3 range, we found a trend for lower lacunar density and increasing 50% cutoff of the

lacunar volume cumulative distribution for diseased samples. In the larger lacunae 900-3000

μm^3 range, we found significantly higher lacunar density and microporosity in the MM group

compared to the MGUS/SMM group. Regarding the shape distribution, the MGUS/SMM

group showed a trend for flatter, more elongated and anisotropic osteocyte lacunae compared

to the control group, though the differences were not statistically significant. Altogether, our

findings suggest that osteocytes in human MM bone disease undergo changes in their lacunae

morphology, which could be an indicator for impaired bone quality. Future studies are

needed to show whether these are consistent within comparable anatomical sites and could

serve as a diagnostic or prognostic marker.

Keywords

Osteocyte lacuna, Morphometry; High resolution microCT; Human bone biopsy; Multiple

myeloma (MM); Monoclonal gammopathy of undetermined significance (MGUS);

Smoldering myeloma (SMM)

1. Introduction

Bone is a dynamic organ which, besides providing structural support to the body, acts as a metabolic and hematopoietic reservoir. In addition to the vast number of cell types and biomolecules involved in the bone organ, bone extracellular matrix (ECM) also plays a crucial role in maintaining bone homeostasis [1]. Bone ECM is composed of an inorganic (hydroxyapatite mineral crystals) and an organic phase (primarily of collagen type I and proteoglycans), which provide mechanical strength. Osteocytes are bone-embedded cells, connected via dendrites in a lacuno-canalicular network (LCN). They act as local sentinels in response to external stimuli and regulate the balance between bone resorption/formation [2]. Hence, factors such as collagen, mineral crystals and osteocyte LCN affecting bone matrix organization will have an impact on bone physiology

Lacunar volume, shape and density has been shown to be influenced by changes of the surrounding environment, either mechanically or chemically, and by aging or disease. Larger lacunae have been observed after exposing mice to non-gravity [3] or after treatment with glucocorticoid to slow down bone metabolism [4]. Smaller lacunar size and density have been observed in rodent models of aging [5]. Significantly lower osteocyte lacunar volume was found in an osteoporotic rat model compared to healthy controls and the effect of different anti-resorptive drugs in intracortical microporosities was evaluated [6]. In humans, decreasing lacunar density was observed with aging, while a significantly higher density was found in osteoporotic bone compared to controls [7]. A recent study with human bone biopsy samples of healthy individuals across the life span revealed decreasing osteocyte lacunae density and porosity with aging before the peak bone mass at 30 years, which then stabilized or even increased after this age [8]. Mineralized osteocyte lacunae (micropetrosis) have been found with aging and osteoporosis, attributed to osteocyte apoptosis, which was improved with bisphosphonates [9]. Lacunar shape changes have also been associated with aging, becoming smaller and more spherical with increasing age [10]. Such osteocyte morphological changes are responsible for lower local bone tissue strains and affect bone mechanosensitivity [11]. In osteogenesis imperfecta, a higher density of osteocyte lacunae per unit volume [12–14], with more spherical shape compared to the ellipsoidal lacunae in control mice was observed [14].

In cancer, osteocytes, as well as osteoblasts and osteoclasts, communicate with tumor cells and this generates a microenvironment that supports cancer cell growth and stimulates bone destruction [15]. Interactions between breast and prostate cancer cells and osteocytes affect the

cancer cell migration and invasion potential and contribute to the establishment and

progression of bone metastasis [16,17]. Also, breast cancer cells induce osteocyte apoptosis and

alter osteocyte function [18]. Recently, a study of osteotropic cancers in rodents revealed that

the spatial distribution of cortical bone microporosity, osteocyte lacunae volume and the LCN

characteristics are influenced by the presence of tumor cells in osteosclerotic and osteolytic

lesions [19]. Taken together, changes in bone microstructure and the LCN play a role in

different types of bone metastasis. Ultrastructural characterization will help understand how

different tumor cells interact with osteocytes, causing characteristic footprints in the bone

microstructure and impairing bone integrity and physiology.

An example of an incurable malignancy of the bone marrow is multiple myeloma (MM), in

which plasma cells disrupt the bone homeostasis towards excessive bone resorption [20].

Patients diagnosed with MM develop symptoms termed CRAB: hypercalcemia, renal

insufficiency, anemia and osteolytic bone lesions[21]. Initially, an abnormal proliferation of

plasma cells (< 10%) producing aberrant antibodies in serum (< 3 g/dL) is clinically

identified as benign, termed 'monoclonal gammopathy of underdetermined significance'

(MGUS). When MGUS continuously progresses into the next stage, named smoldering

multiple myeloma (SMM), CRAB symptoms are not yet present. However, SMM represents

a broad biological spectrum: (i) clinical cases which do not progress into symptomatic

disease over years, and (ii) high-risk cases in which patients have an 80 % chance of disease

progression within two years [22]. To better define those high-risk SMM, who require

immediate intervention to prevent end-organ damage, particularly to bone and kidney, the

International Myeloma Working Group published updated the criteria for the diagnosis of

MM [23]. Validated biomarkers were included, such as the detection of one or more focal

lesions by magnetic resonance imaging (MRI) and diffuse infiltration ($\geq$ 60%) of clonal

plasma cell in the bone marrow even without bone lytic lesions.

MM cells alter the bone marrow environment by releasing signals that promote osteoclast

activity, while inhibiting osteoblast function [24,25]. Interestingly, MM bone lesions rarely heal,

even after years of patients being in complete disease remission [26]. There is evidence that

MM cells also target osteocytes by enhancing cell apoptosis and expression of sclerostin, an

inhibitor of bone formation [27]. Even though MM cells directly interact with osteocytes and

vice versa, the consequences of these interactions on the local bone microstructure and the

role of the ECM in disease development are largely unknown [27]. Our group has shown local

ECM alterations with active erosion sites, irregular shaped osteocyte lacunae and altered

osteocyte LCN architecture, using an early MM mouse model [28]. Thus, examining the bone

microstructure in MM and the precursor conditions MGUS and SMM would provide insights

in the pathophysiology of this disease. It is currently unknown how human bone ECM is

affected at the ultrastructural level in MGUS, SMM and newly diagnosed MM bone disease.

The aim of this study is to quantitatively characterize changes in osteocyte lacunae and

micropores from MGUS to newly diagnosed MM, using ex vivo human bone biopsies.

Determination of these changes could help identifying diagnostic or prognostic indicators for

the progression of MM bone disease.

2. Results

2.1 Clinical data and patient history

Clinical data from patients from the University Hospital Würzburg and parameters describing

bone metabolism are compiled in Tables 1-3. The cohort included patient-derived bone

biopsy samples with the precursor condition MGUS (Table 1), SMM (Table 2), and newly

diagnosed MM (Table 3). The revised International Staging System for Multiple myeloma (r-

ISS) was used to stratify patients with respect to their survival [29]. Control samples obtained

from the University Hospital Würzburg and from the Ludwig Boltzmann-Institute of

Osteology Vienna are compiled in Table 4. Only biopsy samples containing sufficient

trabecular bone were included.

Patients with MGUS showed no detectable osteolytic bone lesions by low-dose CT scans.

One patient with MGUS received denosumab for four months. In this case, we cannot

exclude that the anti-resorptive treatment interfered with the bone ultrastructure. Similarly,

the two patients classified as SMM exhibited no signs of osteolytic lesions by low-dose CT

scans at the time of biopsy. The disease stage of SMM was based on the percent of bone

marrow infiltration of $CD138^+$ cells, above 10%. Patients classified as MM had a bone

marrow infiltration of $CD138^+$ cells between 60-90% (4 out of 6), a ratio of the involved to

the uninvolved free light chain in the serum (sFLC) of >100 (2 out of 6), and/or local or

disseminated lytic lesions, as well as reduced bone mineral density (4 out of 6). All bone

turnover markers (phosphate, calcium, alkaline phosphatase) were within normal ranges.

Anti-resorptive therapy with the bisphosphonate zoledronic acid had been administered to

one MM patient for one month before the biopsy was taken. We assume that the single dose

of the bisphosphonate did not affect bone ultrastructure in such short time.

2.2 Immunohistochemical (IHC) and microcomputed tomography (microCT) overview analysis

As part of the standard clinical practice, bone biopsies were processed for immunohistochemical (IHC) analysis for CD138 staining, to detect the clonal bone marrow plasma cells and quantify the percent of bone marrow infiltration of CD138$^+$ cells. Fig. 1a-c shows representative samples of MGUS, SMM and newly diagnosed MM patients with <10% for MGUS and >10% for SMM and MM patients. Bone biopsy samples containing sufficient trabecular bone were scanned with microcomputed tomography (microCT). 3D renders of representative images are shown in Fig. 1d-f. Quantification of trabecular thickness distribution is shown in Fig. 1g-j. No differences between the three groups were observed in the macroscopic trabecular bone architecture, indicating the resolution might limit the ability to detect pathological changes.

2.3 Bone ultrastructure and segmentation of osteocyte lacunar microporosity

We next investigated the bone ultrastructure with a focus on the osteocyte lacunar microporosity. High resolution microCT scans (voxel size 1-2 μm) were performed on smaller volumes of interest (VOI) and the empty cavities within mineralized tissue corresponding to osteocyte lacunae were segmented. Cavities smaller than 20 μm^3 and larger than 3000 μm^3 were considered cracks or artifacts and excluded from the analysis. VOI of representative samples and the segmented osteocyte lacunar microporosity are visualized in Fig. 2.

2.4. Osteocyte lacunar volume distribution and microporosity analysis

We characterized the osteocyte lacunar volume distribution, first as a frequency distribution (Fig. 3) and then as a cumulative distribution (Fig. 4). To plot the lacunar volume frequency distribution, all lacunae within one sample were stratified according to volume intervals. For a discrete lacunar volume interval, we quantified the number of osteocyte lacunae (Lc.N.) for that given size, normalized to the trabecular bone volume and excluding lacunar total volume (Tb.TV-Lc.TV), to account for samples of different size. Two separate lacunar volume ranges were investigated: small lacunae 20-900 μm³ (Fig. 3a-c) and larger lacunae 900-3000 μm³ (Fig. 3d-f). Control samples (Fig. 3a, d) were compared with MGUS, SMM (Fig. 3b, e), and MM (Fig. 3c, f).

In the small lacunae range 20-900 μm³, we observed a comparable distribution in the

different groups, with the exception of sample #MM 3, with significantly higher number of

osteocyte lacunae compared to other samples within the MM group (Fig. 3c). In contrast, in

the larger lacunae range 900-3000 μm³, we observe a significantly higher number of lacunae

for the MM group (Fig. 3f) compared with MGUS (Fig. 3d) and SMM (Fig. 3e) groups

When comparing both ranges, we observed a larger number of small osteocyte lacunae (Fig.

3a-c) compared to larger lacunae (Fig. 3d-f). This motivated a more detailed lacunar volume

cumulative distribution analysis (Fig. 4), where the lacunar number (Lc.N) was plotted as a

cumulative curve. The 50% cutoff indicates that half of all osteocyte lacunae within one

sample are below that specific volume interval (x-axis). In the control group (Fig. 4a), the

50% cutoff is heterogeneous: samples #control 1, #control 3 and #control 4 have 50% of the

lacunae with volumes around 140-170 μm³, while sample #control 2 has the highest volume

with 270 μm³. In the MGUS/SMM group (Fig. 4b), the 50% cutoff ranges from 170-210

μm³, except sample #SMM 2 with the smallest cutoff at 140 μm³. In the MM group (Fig. 4c),

the 50% cutoff varies from 150-220 μm³, with clearly lower values for the biopsies of

patients without bone osteolytic lesions (#MM 3 and #MM 6). In conclusion, we observe a

trend for increasing 50% cutoff for more advanced disease, indicating that the sum volume of

the smallest 50% lacunae account for a larger volume as the disease progresses (Fig. 4c).

Finally, we calculated the lacunar density as the total number of osteocyte lacunae (Lc.TN)

normalized to the trabecular bone volume and excluding lacunar total volume (Tb.TV-

Lc.TV), in other words, the summation of the osteocyte lacunar volume frequency

distribution (Fig. 3). This was done for both ranges separately, small lacunae 20-900 μm³

(Fig. 5a) and larger lacunae 900-3000 μm³ (Fig. 5b). In the small lacunae range, the mean for

the control samples was 29809 +/- 11314 lacunae/mm³, for MGUS/SMM 18165 +/- 3278

lacunae/mm³ and for MM 20502 +/- 13827 lacunae/mm³. No significant differences were

observed in the small lacunae range, although there was a clear trend for lower lacunar

density for diseased samples (MGUS/SMM and MM) compared to the controls. However, in

the larger lacunae range 900-3000 μm³ (Fig. 5b), significantly higher lacunar density was

found in the MM group compared to the MGUS/SMM group.

We also calculated the microporosity as the lacunar total volume (Lc.TV) divided by

trabecular total bone volume (Tb.TV) for each group. This was done for both ranges

separately, small lacunae 20-900 µm³ (Fig. 5c) and larger lacunae 900-3000 µm³ (Fig. 5d).

No significant differences were observed in the small lacunae range. However, in the larger

lacunae range, significantly higher microporosity was found in the MM group compared to

the MGUS/SMM group. This is consistent with the observations of lacunar volume frequency

distribution (Fig. 3f) and lacunar density (Fig. 5b).

2.5 Osteocyte lacunar morphological analysis

We performed a lacunar morphological analysis in the small lacunae 20-900 µm³ range, for

each group control, MGUS/SMM and newly diagnosed MM. Based on previous analogous

analysis [30,31], we investigated the distribution of lacunar flatness, elongation and anisotropy.

To do so, the principal eigenvalues for each osteocyte lacunae were obtained: EV1, EV2 and

EV3. The morphological parameters were calculated as follows: lacuna elongation as

EV2/EV1 (ratio of medium to largest eigenvalue) ranging from lower values for elongated

and 1 for spherical (Fig. 6a-d); lacuna flatness as EV3/EV2 (ratio of smallest to medium

eigenvalue) ranging from 0 for flat to 1 for spherical (Fig. 6e-h); and lacuna anisotropy as 1-

EV3/EV1 (one minus the ratio of smallest to largest eigenvalue) ranging from 0 for

isotropic/spherical to 1 for highest anisotropy (Fig. 6i-l). The fraction of lacunar number

(Lc.N) normalized against lacunae total number (Lc.TN) in each sample is shown for each

group control (Fig. 6a, e, i), MGUS/SMM (Fig. 6b, f, j) and MM (Fig. 6c, g, k). The median

of all lacuna elongation values for each sample are shown in Fig. 6d; similarly, for flatness in

Fig. 6h and anisotropy in Fig. 6l.

Lacuna flatness in MGUS/SMM and newly diagnosed MM groups exhibit a broader spread

of the distribution compared to the control group, with a shift towards lower values (flatter

shapes). Regarding lacuna elongation and anisotropy, the spread of the distribution for the

three groups is comparable. A trend for lower values for lacuna elongation (more elongated)

and higher values for lacuna anisotropy (more anisotropic) is observed in the MGUS/SMM

group compared to the control group, as shown by the curves and the by the median values.

However, the differences of the median values are not significant.

3. Discussion

Osteocyte function is altered in skeletal disorders including cancer. In MM bone disease, osteolytic lesions are frequently diagnosed in clinical CT scans, however, changes in the mineralized ECM and morphometric analyses of bone microporosity in bone biopsies are not routinely analyzed. To our knowledge, here we present the first quantitative investigation of osteocyte lacunae volume and shape distribution in human bone biopsy samples obtained from MGUS, SMM and newly diagnosed MM patients using high resolution microCT (voxel size 1-2 μm).

Our data demonstrate altered lacunae volume and shape distribution with MGUS, SMM and newly diagnosed MM. Specifically, we found a significantly higher number of larger lacunae in the 900-3000 μm³ range in the MM group compared to the MGUS/SMM groups, as reflected in an increase in lacunar volume frequency distribution (Fig. 3f) and lacunar density (Fig. 5b). The study also found significantly higher microporosity for the larger lacunae range in the MM group compared to the MGUS/SMM group (Fig. d), consistent with the observation of an increase in lacunar volume frequency distribution. One limitation of this analysis is that the larger lacunae in the 900-3000 μm³ range probably includes both enlarged osteocyte lacunae and other pathological features in the form of micropores.

In the small lacunae 20-900 μm³ range, the lacunar density for control samples with 29809 +/- 11314 lacunae/mm³ (Fig. 5a) is in the range previously reported in the literature for 3D analysis of osteocyte morphometry in healthy transiliac bone biopsies [32], which confirms the validity of our analysis. Interestingly, there was a trend for lower lacunar density for diseased samples (MGUS/SMM and MM) compared to the controls, though the differences were not significant (Fig. 5a). This could be indicative of micropetrosis, i.e. osteocyte lacunae mineralization following osteocyte apoptosis [33,34]. Since a lower lacunar density can distinguish healthy, osteoporotic and bisphosphonate-treated osteoporotic patients, it is currently being considered as a novel bone microstructural maker of impaired bone quality [33]. Finally, we observed a trend for increasing values of the 50% cutoff in the lacunar volume cumulative distribution for more advanced disease, showing that the sum volume of the smallest 50% lacunae account for a larger volume as the disease progresses (Fig. 4).

In terms of shape distribution, the MGUS/SMM group showed a trend for lower lacuna flatness (flatter), lower lacuna elongation (more elongated), and higher lacuna anisotropy

(more anisotropy) compared to the control group (Fig. 6). Altogether, the findings of a trend

for lower lacunar density and increasing 50% cutoff of the lacunar volume cumulative

distribution for diseased samples in the small lacunae 20-900 μm^3 range, together with

significantly higher lacunar density and microporosity for the MM group in the larger lacunae

900-3000 μm^3 range, suggest that the osteocytes in MM bone disease and the precursor

conditions MGUS/SMM are undergoing changes in their lacunae morphology.

In a recent study in immunocompetent mice, breast and prostate cancer cells were

intratibially injected and the changes in the osteocyte LCN induced by tumor cells were

analyzed by histology, microCT imaging and confocal laser scanning microscopy [27].

Interestingly, large lacunae and vascular canals were not observed in the proximity of

osteolytic lesions, whereas these changes occurred in osteosclerotic lesions adjacent to

prostate cancer cells [27], indicating that changes of osteocyte LCN characteristics are tumor

type-specific. In our study of biopsy samples from patients with MM and the precursor

conditions, we observed a significantly higher number of larger lacunae in the MM group

compared to the MGUS/SMM groups. These changes may be related to the presence of

osteocytic osteolysis [35], a process that involves osteocytes mobilizing calcium and phosphate,

using carbonic anhydrase and vacuolar ATPase to demineralize the bone matrix, and digest

protein using matrix metalloproteases and tartrate-resistant acid phosphatase (TRAP) [27,36–38].

In the above-mentioned mouse model [27], TRAP-positive osteocytes in combination with large

lacunae were detected in osteosclerotic regions of breast and prostate infiltrated bones,

indicating that this mechanism could contribute to the observed increase in lacunae volume

[27,36–38]. Whether osteocytic osteolysis plays a role in the progression from healthy to

MGUS/SMM to MM bone is not known and warrants further studies. Moreover, since the

osteocyte remodeling function affects the lacunae morphology and the LCN architecture, it is

likely that changes in the latter are indicators for impaired bone remodeling activity.

In order to understand the implications of altered lacunae volume and shape distribution in

MM, future studies should consider several factors. First, there is a need for more bone

biopsies of sufficient quality to obtain a larger sample size and validate the findings of this

study. Second, it is important that the bone biopsies are obtained from comparable anatomical

sites to minimize the natural osteocyte volume and shape variation within healthy bone [8,32,39].

Additionally, to further investigate the relationship between osteocyte lacunae and MM,

researchers should increase the volume of interest scanned at high resolution (1 μm voxel

size or lower) for instance using phase-contrast synchrotron microCT. Furthermore, the

implementation of deep learning algorithms could facilitate the analysis of large numbers of

osteocyte lacunae and improve the accuracy of image analysis. In addition to lacunar

abnormalities, quantitative analysis of alterations in the LCN (i.e. canalicular density,

connectivity) should be explored in future studies. Finally, investigating clinical bone

endocrine parameters such as parathyroid hormone, bone-specific alkaline phosphatase,

amino-terminal pro-peptide of type I procollagen, carboxy-terminal telopeptide of type I

collagen, TRAP5b or fibroblast growth factor-23 produced by osteocytes, in relation to

calcium and phosphorus and in relation to lacunae morphology, could provide valuable

insights into the pathogenesis of MM and link this to the clinical setting [40]. Measuring serum

parameters may be easier than performing microCT analysis of osteocyte lacuna, and

incorporating these measurements into future studies could provide a more comprehensive

understanding of the impaired bone remodeling capacity in MM bone disease. Additionally,

the use of animal models of MM and other bone diseases may provide a valuable tool for

investigating the mechanisms underlying the observed alterations in osteocyte lacunae

morphology and other aspects of bone ultrastructure, such as LCN architecture, bone

composition, and micro- and nanoscale organization of the organic and inorganic matrix. We

recently established a MM bone disease model for ultrastructural characterization of the ECM

in early stages of the disease [28,41–43]. In skeletally mature mice, we detected a disorganized

osteocyte LCN architecture, and irregular-shaped osteocyte lacunae in MM-injected bones

after 21 days [28]. This model will help to characterize early on the development and

progression of ultrastructural changes of MM bone disease.

Taken together, these findings suggest that altered lacunae volume and shape distribution

may play a role in the pathogenesis of MM and the precursor conditions MGUS and SMM,

and could potentially serve as a diagnostic or prognostic marker for the disease. Further

studies are needed to explore the clinical implications of these results and to determine

whether targeting lacunar abnormalities could be a viable therapeutic approach for MM.

4. Materials and methods

4.1 Patient sample collection and clinical evaluation

The purpose of this study was to determine whether changes in osteocyte lacunae volume and

shape distribution could be detected in mineralized bone biopsy samples from patients with

MGUS, SMM and newly diagnosed MM. MGUS (n=3), SMM (n=2) and symptomatic MM (n=6) were diagnosed following the revised international staging system [23]. Clinical data from patients including reports of the low-dose CT scans are given in Tables 1-3. The investigators who performed the bench studies were blind to the patient information. This study was approved by the Ethics Committee of the University of Würzburg, Germany (82/20-am).

As control bone biopsy samples, two different data sets were used (Table 4). One Jamshidi bone biopsy sample (2 mm diameter) was obtained from a patient of the University Hospital Würzburg with myelodysplastic syndrome. Three samples (5 mm diameter) were obtained from an earlier study [8] from autopsies at the Ludwig Boltzmann-Institute of Osteology Vienna. Osteocyte lacunae characteristics were re-evaluated in the current study. For all control and disease bone biopsy samples, the trabecular bone compartment was analyzed and the cortical bone was excluded. Only biopsy samples containing sufficient trabecular bone were considered.

The patient clinical data (Tables 1-3) include: biopsy number, disease stage (MGUS, SMM or newly diagnosed MM), age, gender, immunoglobulin subtypes (heavy and light chains) secreted by malignant plasma cells, revised International Staging System (r-ISS), cytogenetic risk, M-protein secreted by plasma cells at time of diagnosis (g/L), heavy chain (mg/dL), involved serum free light chain (sFLC) (mg/L), ratio (involved/uninvolved sFLC), bone marrow infiltration (%) based on immunohistochemistry Syndecan-1 (CD138) with >60% corresponding to newly diagnosed MM, computed tomography findings of osteolytic lesions, hemoglobin (g/dL), creatinine (mg/dL) and cytogenetic alterations by fluorescence in situ hybridization (FISH), which allows for detection of genetic changes which are relevant for the ISS stage. In addition, parameters describing the bone metabolism include: calcium (mmol/L), alkaline phosphatase (U/L), phosphate (mmol/L) and finally, bone anti-resorption treatment ongoing at the time of biopsy.

4.2 Immunohistochemical detection of CD138 on decalcified bone paraffin sections
Paraffin embedded human specimens were retrospectively collected from formalin-fixed paraffin-embedded tissue of anonymized samples, archived at the Institute of Pathology, University of Würzburg. Shortly, Jamshidi bone biopsy samples that were derived from the clinical department of the University of Würzburg were fixed for 24 h in formalin,

decalcified for 24 h at 37°C using an EDTA-based approach, dehydrated with alcohol and

xylene and then embedded in paraffin.

For the immunohistochemical detection of CD138/Syndecan-1 expression, sections were

deparaffinized. The tissue was hybridized with an antibody against CD138/Syndecan-1

(clone MI15, mouse, #M7228, Agilent, Santa Clara, CA, USA), following standard

procedures by automated processing using the Tecan Evo Freedom stainer and the Dako

Advance system according to the manufacturer's protocol.

4.3 Microcomputed tomography (microCT): image acquisition

Specimens were scanned using an EasyTom micro/nano tomograph (RX solutions, France).

Low resolution scanning parameters were: 107 kV, 93 µA, 7 µm voxel size, frame rate of 3,

average frame of 5. High resolution scanning parameters were: 60 kV, 124 µA, 1-2 µm voxel

size, frame rate of 1, average frame of 5. Reconstruction of the 1120 projections/scan were

performed using RX Solutions X-Act software.

4.4 Low resolution microCT: image analysis

The overall bone biopsy morphology with particular focus on trabecular bone thickness was

analyzed with Dragonfly v.2022.1 software (Object Research Systems Inc., Montreal,

Canada, 2022). Low resolution microCT stack images (voxel size of 7 µm) were segmented

using Otsu thresholding ("denoising" of these microCT images and objects was not

necessary). A mesh was then created from each individual region of interest (ROI) of the

trabecular bone.

The trabecular bone strut thickness was automatically measured from each mesh by

Dragonfly software. For this, we calculated the mean and standard deviation values of about

3-5.5 10^6 local vertices created between boundary points of each overall mesh. The software

calculated these vertices as diameters of hypothetical spheres that fit within each boundary

points of the mesh. The trabecular bone strut thickness distribution is depicted with a color

code for each biopsy and as a histogram.

4.5 High resolution microCT: image analysis

<u>4.5.1 Segmentation of osteocyte lacunae</u>

The stack of high resolution microCT images (1-2 μm voxel size) was segmented using Otsu

thresholding in Dragonfly. For these images, noise removal was performed using 3D

smoothing (kernel of 3) as morphological operation. Next, the binary mask was used to

extract the pores. Osteocyte lacunae were filled in a copy of the binary mask using a filling

morphological operation. Next, the multi-ROI conversion tool of Dragonfly was used to

select each lacuna individually. This tool allowed to define each osteocyte lacuna as an

individual ROI, hence enabling the calculation of each lacunae volume and shape. The

generated binary images were then used for the quantitative analysis of lacunae volume and

shape with Python software (version 3.5). The script used was written in a Jupyter notebook

with Python software (version 3.7). External libraries not contained in the Anaconda

environment were installed from their repository. Micropores smaller than 20 μm^3 and larger

than 3000 μm^3 were considered cracks or artifacts and excluded from the analysis. Two

separate lacunar volume ranges were investigated: small lacunae 20-900 μm^3 [44] and larger

lacunae 900-3000 μm^3.

<u>4.5.2 Osteocyte lacunar volume analysis</u>

For the osteocyte lacunar volume analysis, each segmented lacunar volume was calculated as

the total number of voxels times the volume of a single voxel. Based on this, we could define

the number of lacunae (Lc.N) of a given lacunar volume (Lc.V). We could also define the

total number of osteocyte lacunae (Lc.TN), total lacunar volume (Lc.TV) and trabecular bone

volume (Tb.BV). This nomenclature and units are summarized in Table 5.

<u>4.5.3 Normalized lacunar volume frequency distribution and lacunar density</u>

The lacunar volume frequency distributions were normalized to the trabecular bone volume

to account for size differences between samples, since larger samples have more lacunae than

smaller ones. For a given lacunar volume (Lc.V), we quantified the lacunar number (Lc.N),

normalized to the trabecular bone volume (Tb.BV) and excluding the total lacunar volume

(Tb.TV-Lc.TV). The data is presented as the frequency in a histogram with a bin size of

20 μm^3. Furthermore, the lacunar density was calculated as the total number of osteocyte

lacunae (Lc.TN) normalized to the trabecular bone volume and excluding lacunar total

volume (Tb.TV-Lc.TV), in other words, the summation of the osteocyte lacunar volume

frequency distribution. This was done for both ranges separately, small lacunae 20-900 μm^3

and larger lacunae 900-3000 μm^3.

4.5.4 Lacunar volume cumulative distribution

The cumulative distribution is calculated by sorting all osteocyte lacunae by volume, from

smallest to largest, and increasing the count of the fraction 1/N at each point, with N = length

of array. The cumulative lacunae volume distribution was plotted with respect to the lacunae

volume (Lc.V), with the x axis showing a given lacunae volume and the y axis showing the

cumulative volume. The 50% cutoff illustrating the specific volume below which half of all

osteocyte lacunae are contained, was marked with a dashed line.

4.5.5 Osteocyte lacunar microporosity analysis

The microporosity was calculated as the lacunar total volume (Lc.TV) divided by trabecular

total bone volume (Tb.TV) for each group. This was done for both ranges separately, small

lacunae 20-900 μm^3 and larger lacunae 900-3000 μm^3.

4.5.6 Osteocyte lacunar morphological analysis

To perform the lacunar morphological analysis, we defined the eigenvectors of an individual

lacuna with the corresponding major and minor axes. From the eigenvectors, the

corresponding eigenvalues (EV) were derived (EV1 > EV2 > EV3), where EV1 is the largest

eigenvalue and EV3 the smallest [45,46]. Three parameters were assessed to examine lacunae

morphology, based on the eigenvalues of each individual lacuna: the lacuna elongation,

flatness and anisotropy [30,31]. This nomenclature and units are summarized in Table 6.

4.6 Statistical analysis

A total of n=15 bone biopsy samples were analyzed, including MGUS n=3, SMM n=2, newly

diagnosed MM n=6 and control biopsy samples n=4 (Jamshidi n=1 and from autopsies n=3).

Additional bone biopsy samples (n>15) were collected but excluded from the analysis due to

lack of sample integrity (e.g. loss of bone structure (bone debris) during the extraction

procedure) or insufficient trabecular bone. To analyze changes in bone microporosity and

lacunar morphological analysis, a one-way analysis of variance (ANOVA) with Tukey's

multiple comparisons test (*p<0.05) was used (GraphPad Prism 8.0 software).

5. Conflict of interest

484 The authors declare no conflict of interest.

6. Data availability

The raw/processed data required to reproduce these findings are available in a publicly accessible repository of the Max Planck Society.

7. Author contributions

A Cipitria, I. Moreno-Jiménez and F. Jundt conceived the idea. I. Moreno-Jiménez and S. Heinig processed the bone biopsy samples and performed the experiments. D. Maichl collected and prepared the human Jamshidi bone biopsy samples. S. Strifler educated patients about and performed the biopsies, and collected clinical data. E. Leich-Zbat collected the human bone biopsy samples and clinical data; S. Blouin provided the control bone autopsy samples. I. Moreno-Jiménez, S. Heinig, U. Heras, F. Jundt and A. Cipitria analyzed the data. P. Fratzl and N. Fratzl-Zelman together with A Cipitria, I. Moreno-Jiménez and F. Jundt evaluated the methods and results. A Cipitria, I. Moreno-Jiménez and F. Jundt drafted the manuscript. All authors discussed the results and contributed to the final manuscript.

8. Funding

This research was funded by a postdoctoral research fellowship from the Humboldt Foundation (I.M.-J.) and by the Deutsche Forschungsgemeinschaft (DFG) Emmy Noether grant CI 203/2-1 (A.C). This work was supported by the Interdisciplinary Center for Clinical Research (IZKF), Medical Faculty of Würzburg, grant B-409 (F.J.) and the German Research Foundation (DFG) grants JU426/10-1 (F.J., 491715122) and JU 426/11-1 (F.J., 496963451). A.C. also thanks the funding from IKERBASQUE Basque Foundation for Science and from the Spanish Ministry of Science and Innovation (PID2021-123013OB-I00) (Ministerio de Ciencia e Innovación, la Agencia y del Fondo Europeo de Desarrollo Regional, Proyecto PID2021-123013OB-I00 financiado por MCIN/AEI/10.13039/501100011033/FEDER.UE).

9. Acknowledgements

The authors thank Daniel Werner, Jeannette Steffen, Daniela Garske and Susann Weichold at the Max Planck Institute of Colloids and Interfaces in Potsdam for their technical assistance.

References

1. Fratzl, P. & Weinkamer, R. Nature's hierarchical materials. *Prog Mater Sci* **52,** 1263–1334 (2007).
2. Bonewald, L. F. The amazing osteocyte. *Journal of Bone and Mineral Research* **26,** 229–238 (2011).

521   3.   Gerbaix, M., Gnyubkin, V., Farlay, D., Olivier, C., Ammann, P., Courbon, G.,
522   Laroche, N., Genthial, R., Follet, H., Peyrin, F., Shenkman, B., Gauquelin-Koch, G. &
523   Vico, L. One-month spaceflight compromises the bone microstructure, tissue-level
524   mechanical properties, osteocyte survival and lacunae volume in mature mice
525   skeletons. *Sci Rep* **7,** 2659 (2017).
526   4.   Lane, N. E., Yao, W., Balooch, M., Nalla, R. K., Balooch, G., Habelitz, S., Kinney, J.
527   H. & Bonewald, L. F. Glucocorticoid-treated mice have localized changes in
528   trabecular bone material properties and osteocyte lacunar size that are not observed in
529   placebo-treated or estrogen-deficient mice. *Journal of Bone and Mineral Research* **21,**
530   466–476 (2005).
531   5.   Tiede-Lewis, L. M. & Dallas, S. L. Changes in the osteocyte lacunocanalicular
532   network with aging. *Bone* **122,** 101–113 (2019).
533   6.   Tommasini, S. M., Trinward, A., Acerbo, A. S., De Carlo, F., Miller, L. M. & Judex,
534   S. Changes in intracortical microporosities induced by pharmaceutical treatment of
535   osteoporosis as detected by high resolution micro-CT. *Bone* **50,** 596–604 (2012).
536   7.   Mullender, M. G., van der Meer, D. D., Huiskes, R. & Lips, P. Osteocyte density
537   changes in aging and osteoporosis. *Bone* **18,** 109–113 (1996).
538   8.   Blouin, S., Misof, B. M., Mähr, M., Fratzl-Zelman, N., Roschger, P., Lueger, S.,
539   Messmer, P., Keplinger, P., Rauch, F., Glorieux, F. H., Berzlanovich, A., Gruber, G.
540   M., Brugger, P. C., Shane, E., Recker, R. R., Zwerina, J. & Hartmann, M. A.
541   Osteocyte lacunae in transiliac bone biopsy samples across life span. *Acta Biomater*
542   **157,** 275–287 (2023).
543   9.   Milovanovic, P., Zimmermann, E. A., Riedel, C., Scheidt, A. vom, Herzog, L., Krause,
544   M., Djonic, D., Djuric, M., Püschel, K., Amling, M., Ritchie, R. O. & Busse, B. Multi-
545   level characterization of human femoral cortices and their underlying osteocyte
546   network reveal trends in quality of young, aged, osteoporotic and antiresorptive-treated
547   bone. *Biomaterials* **45,** 46–55 (2015).
548   10.   Hemmatian, H., Bakker, A. D., Klein-Nulend, J. & van Lenthe, G. H. Aging,
549   osteocytes, and mechanotransduction. *Curr Osteoporos Rep* **15,** 401–411 (2017).
550   11.   Hemmatian, H., Bakker, A. D., Klein-Nulend, J. & van Lenthe, G. H. Alterations in
551   osteocyte lacunar morphology affect local bone tissue strains. *J Mech Behav Biomed*
552   *Mater* **123,** 104730 (2021).
553   12.   Mähr, M., Blouin, S., Behanova, M., Misof, B. M., Glorieux, F. H., Zwerina, J.,
554   Rauch, F., Hartmann, M. A. & Fratzl-Zelman, N. Increased Osteocyte Lacunae
555   Density in the Hypermineralized Bone Matrix of Children with Osteogenesis
556   Imperfecta Type I. *Int J Mol Sci* **22,** 4508 (2021).
557   13.   Hedjazi, G., Guterman-Ram, G., Blouin, S., Schemenz, V., Wagermaier, W., Fratzl, P.,
558   Hartmann, M. A., Zwerina, J., Fratzl-Zelman, N. & Marini, J. C. Alterations of bone
559   material properties in growing Ifitm5/BRIL p.S42 knock-in mice, a new model for
560   atypical type VI osteogenesis imperfecta. *Bone* **162,** 116451 (2022).
561   14.   Carriero, A., Doube, M., Vogt, M., Busse, B., Zustin, J., Levchuk, A., Schneider, P.,
562   Müller, R. & Shefelbine, S. J. Altered lacunar and vascular porosity in osteogenesis
563   imperfecta mouse bone as revealed by synchrotron tomography contributes to bone
564   fragility. *Bone* **61,** 116–124 (2014).
565   15.   Atkinson, E. G. & Delgado-Calle, J. The emerging role of osteocytes in cancer in
566   bone. *JBMR Plus* **3,** e10186 (2019).
567   16.   Adhikari, M. & Delgado-Calle, J. Role of osteocytes in cancer progression in the bone
568   and the associated skeletal disease. *Curr Osteoporos Rep* **19,** 247–255 (2021).

569   17.   Hofbauer, L. C., Bozec, A., Rauner, M., Jakob, F., Perner, S. & Pantel, K. Novel
570   approaches to target the microenvironment of bone metastasis. *Nat Rev Clin Oncol* **18,**
571   488–505 (2021).
572   18.   Mastro, A. M., Gay, C. V., Welch, D. R., Donahue, H. J., Jewell, J., Mercer, R.,
573   DiGirolamo, D., Chislock, E. M. & Guttridge, K. Breast cancer cells induce osteoblast
574   apoptosis: A possible contributor to bone degradation. *J Cell Biochem* **91,** 265–276
575   (2004).
576   19.   Hemmatian, H., Conrad, S., Furesi, G., Mletzko, K., Krug, J., Faila, A. V., Kuhlmann,
577   J. D., Rauner, M., Busse, B. & Jähn-Rickert, K. Reorganization of the osteocyte
578   lacuno-canalicular network characteristics in tumor sites of an immunocompetent
579   murine model of osteotropic cancers. *Bone* **152,** 116074 (2021).
580   20.   Roodman, G. Pathogenesis of myeloma bone disease. *Blood Cells Mol Dis* **32,** 290–
581   292 (2004).
582   21.   Huston, A. & Roodman, G. D. Role of the microenvironment in multiple myeloma
583   bone disease. *Future Oncology* **2,** 371–378 (2006).
584   22.   Jacobsen, R. B. & Pharm, D. Diagnosis of smoldering multiple myeloma the TEMPI
585   syndrome — A novel multisystem disease. *New England Journal of Medicine* 2011–
586   2012 (2011).
587   23.   Rajkumar, S. V., Dimopoulos, M. A., Palumbo, A., Blade, J., Merlini, G., Mateos, M.-
588   V., Kumar, S., Hillengass, J., Kastritis, E., Richardson, P., Landgren, O., Paiva, B.,
589   Dispenzieri, A., Weiss, B., LeLeu, X., Zweegman, S., Lonial, S., Rosinol, L.,
590   Zamagni, E., Jagannath, S., Sezer, O., Kristinsson, S. Y., Caers, J., Usmani, S. Z.,
591   Lahuerta, J. J., Johnsen, H. E., Beksac, M., Cavo, M., Goldschmidt, H., Terpos, E.,
592   Kyle, R. A., Anderson, K. C., Durie, B. G. M. & Miguel, J. F. S. International
593   myeloma working group updated criteria for the diagnosis of multiple myeloma.
594   *Lancet Oncol* **15,** e538–e548 (2014).
595   24.   Berenson, J., Rajdev, L. & Broder, M. Bone complications in multiple myeloma.
596   *Cancer Biol Ther* **5,** 1082–1085 (2006).
597   25.   Terpos, E., Ntanasis-Stathopoulos, I. & Dimopoulos, M. A. Myeloma bone disease:
598   from biology findings to treatment approaches. *Blood* **133,** 1534–1539 (2019).
599   26.   Callander, N. S. & Roodman, G. D. Myeloma bone disease. *Semin Hematol* **38,** 276–
600   285 (2001).
601   27.   Delgado-Calle, J., Anderson, J., Cregor, M. D., Hiasa, M., Chirgwin, J. M., Carlesso,
602   N., Yoneda, T., Mohammad, K. S., Plotkin, L. I., Roodman, G. D. & Bellido, T.
603   Bidirectional notch signaling and osteocyte-derived factors in the bone marrow
604   microenvironment promote tumor cell proliferation and bone destruction in multiple
605   myeloma. *Cancer Res* **76,** 1089–1100 (2016).
606   28.   Ziouti, F., Soares, A. P., Moreno-Jiménez, I., Rack, A., Bogen, B., Cipitria, A.,
607   Zaslansky, P. & Jundt, F. An early myeloma bone disease model in skeletally mature
608   mice as a platform for biomaterial characterization of the extracellular matrix. *J Oncol*
609   **2020,** 1–12 (2020).
610   29.   Palumbo, A., Avet-Loiseau, H., Oliva, S., Lokhorst, H. M., Goldschmidt, H., Rosinol,
611   L., Richardson, P., Caltagirone, S., Lahuerta, J. J., Facon, T., Bringhen, S., Gay, F.,
612   Attal, M., Passera, R., Spencer, A., Offidani, M., Kumar, S., Musto, P., Lonial, S.,
613   Petrucci, M. T., Orlowski, R. Z., Zamagni, E., Morgan, G., Dimopoulos, M. A., Durie,
614   B. G. M., Anderson, K. C., Sonneveld, P., San Miguel, J., Cavo, M., Rajkumar, S. V.
615   & Moreau, P. Revised International Staging System for Multiple Myeloma: A Report
616   From International Myeloma Working Group. *Journal of Clinical Oncology* **33,** 2863–
617   2869 (2015).

30. El Bialy, I., Jiskoot, W. & Reza Nejadnik, M. Formulation, delivery and stability of
bone morphogenetic proteins for effective bone regeneration. *Pharm Res* **34,** 1152–
1170 (2017).

31. Chaumel, J., Schotte, M., Bizzarro, J. J., Zaslansky, P., Fratzl, P., Baum, D. & Dean,
M. N. Co-aligned chondrocytes: Zonal morphological variation and structured
arrangement of cell lacunae in tessellated cartilage. *Bone* **134,** 115264 (2020).

32. Goff, E., Cohen, A., Shane, E., Recker, R. R., Kuhn, G. & Müller, R. Large-scale
osteocyte lacunar morphological analysis of transiliac bone in normal and osteoporotic
premenopausal women. *Bone* **160,** 116424 (2022).

33. Milovanovic, P. & Busse, B. Phenomenon of osteocyte lacunar mineralization:
indicator of former osteocyte death and a novel marker of impaired bone quality?
Endocr Connect **9,** R70–R80 (2020).

34. Delgado-Calle, J., Bellido, T. & Roodman, G. D. Role of osteocytes in multiple
myeloma bone disease. *Curr Opin Support Palliat Care* **8,** 407–413 (2014).

35. Tsourdi, E., Jähn, K., Rauner, M., Busse, B. & Bonewald, L. F. Physiological and
pathological osteocytic osteolysis. *J Musculoskelet Neuronal Interact* **18,** 292–303
(2018).

36. Jähn, K., Kelkar, S., Zhao, H., Xie, Y., Tiede-Lewis, L. M., Dusevich, V., Dallas, S. L.
& Bonewald, L. F. Osteocytes acidify their microenvironment in response to PTHrP in
vitro and in lactating mice in vivo. *Journal of Bone and Mineral Research* **32,** 1761–
1772 (2017).

37. Kogawa, M., Wijenayaka, A. R., Ormsby, R. T., Thomas, G. P., Anderson, P. H.,
Bonewald, L. F., Findlay, D. M. & Atkins, G. J. Sclerostin regulates release of bone
mineral by osteocytes by induction of carbonic anhydrase 2. *Journal of Bone and*
Mineral Research **28,** 2436–2448 (2013).

38. Tang, S. Y., Herber, R.-P., Ho, S. P. & Alliston, T. Matrix metalloproteinase-13 is
required for osteocytic perilacunar remodeling and maintains bone fracture resistance.
Journal of Bone and Mineral Research **27,** 1936–1950 (2012).

39. Schemenz, V., Gjardy, A., Chamasemani, F. F., Roschger, A., Roschger, P.,
Zaslansky, P., Helfen, L., Burghammer, M., Fratzl, P., Weinkamer, R., Brunner, R.,
Willie, B. M. & Wagermaier, W. Heterogeneity of the osteocyte lacuno-canalicular
network architecture and material characteristics across different tissue types in
healing bone. *J Struct Biol* **212,** 107616 (2020).

40. Vlot, M. C., den Heijer, M., de Jongh, R. T., Vervloet, M. G., Lems, W. F., de Jonge,
R., Obermayer-Pietsch, B. & Heijboer, A. C. Clinical utility of bone markers in
various diseases. *Bone* **114,** 215–225 (2018).

41. Schwarzer, R., Nickel, N., Godau, J., Willie, B. M., Duda, G. N., Schwarzer, R.,
Cirovic, B., Leutz, A., Manz, R., Bogen, B., Dörken, B. & Jundt, F. Notch pathway
inhibition controls myeloma bone disease in the murine MOPC315.BM model. *Blood*
Cancer J **4,** e217–e217 (2014).

42. Rummler, M., Ziouti, F., Bouchard, A. L., Brandl, A., Duda, G. N., Bogen, B.,
Beilhack, A., Lynch, M. E., Jundt, F. & Willie, B. M. Mechanical loading prevents
bone destruction and exerts anti-tumor effects in the MOPC315.BM.Luc model of
myeloma bone disease. *Acta Biomater* **119,** 247–258 (2021).

43. Ziouti, F., Rummler, M., Steyn, B., Thiele, T., Seliger, A., Duda, G. N., Bogen, B.,
Willie, B. M. & Jundt, F. Prevention of bone destruction by mechanical loading is not
enhanced by the Bruton's tyrosine kinase inhibitor CC-292 in myeloma bone disease.
Int J Mol Sci **22,** 3840 (2021).

44.   McCreadie, B. R., Hollister, S. J., Schaffler, M. B. & Goldstein, S. A. Osteocyte
lacuna size and shape in women with and without osteoporotic fracture. *J Biomech* **37,**
563–572 (2004).
45.   Gescheidtova, E., Marcon, P., Bartusek, K., Gescheidtová, E., Marcon, P. & Bartusek,
K. Visualization of plant fibres via diffusion tensor imaging. in *PIERS Proceedings,*
Suzhou, China (2011).
46.   Mader, K. S., Schneider, P., Müller, R. & Stampanoni, M. A quantitative framework
for the 3D characterization of the osteocyte lacunar system. *Bone* **57,** 142–154 (2013).
674
675

Figures and captions

Figure 1

Figure 1. Immunohistochemical (IHC) CD138 staining and low resolution microCT
overview of the bone biopsies from patients with: (a, d, g) monoclonal gammopathy of
undetermined significance (MGUS), (b, e, h) smoldering myeloma (SMM), and (c, f, i)
newly diagnosed multiple myeloma (MM). (a-c) Representative light microscopy images of
the bone marrow compartment from the biopsy samples: CD138 positive staining in brown,
cell nuclei counterstain in blue. (d-f) 3D renders of low resolution (7 μm voxel) microCT
scans of representative bone biopsies. (g-i) Quantitative analysis of trabecular bone strut
thickness distribution and color code visualization with Dragonfly software. (j) Frequency
distribution of strut thickness. Scale bars equal to 100 μm (a-c), 1 mm (d-f).
688

Figure 2

Figure 2. Bone biopsy macroscopic structure and osteocyte lacunar microporosity

visualized with high resolution microCT. (a-c) 3D rendering of local scans (high resolution

microCT; voxel size 1-2 μm) and (d-f) the corresponding segmented osteocyte lacunar

microporosity of representative samples: (a, d, g) MGUS bone biopsy #MGUS 2, (b, e, h)

SMM bone biopsy #SMM 1, (c, f, i) MM bone biopsy #MM 1. Scale bars equal to 250 μm (a,

d), 350 μm (b, e), 400 μm (c, f) and 20 μm (g-i).

Figure 3

Figure 3. Lacunar volume frequency distribution. Frequency distribution normalized to trabecular bone volume for two separate lacunar volume ranges: 20-900 μm³ and 900-3000 μm³. For each lacunae volume interval (x-axis), number of osteocyte lacunae (Lc.N) normalized by the trabecular total bone volume excluding lacunar total volume (Tb.TV-Lc-TV) (y-axis). Frequency distribution for each group: (a, d) control, (b, e) MGUS and SMM, (c, f) MM. Sample from the Jamshid biopsy in black, all other control samples in grey. MGUS in blue, SMM in green, MM samples with bone lytic lesion in red, MM samples without lytic lesions in orange.

Figure 4

Figure 4. Lacunar volume cumulative distribution for the small lacunae 20-900 µm³

range. Cumulative distribution (from 0 to 1) of lacunae (y-axis) for each volume in µm³ (x-

axis). Cumulative distribution for each group: (a) control, (b) MGUS and SMM, (c) MM.

Dashed line indicates the 50% cutoff volume below which are half of all osteocyte lacunae of

one sample. Sample from the Jamshid biopsy in black, all other control samples in grey.

MGUS in blue, SMM in green, MM samples with bone lytic lesion in red, MM samples

without lytic lesions in orange.

 Figure 5

Figure 5. Lacunar density and microporosity analysis for the small lacunae 20-900 µm³ range and for the larger lacunae 900-3000 µm³ range. Lacunar density calculated as the total number of osteocyte lacunae (Lc.TN) normalized to the trabecular bone volume and excluding lacunar total volume (Tb.TV-Lc.TV), for each group control, MGUS/SMM and newly diagnosed MM (samples with bone lytic lesion in red, samples without lytic lesions in orange). Microporosity calculated as lacunar total volume (Lc.TV) divided by trabecular total bone volume (Tb.TV) for each group. Error bars indicate mean ± SD. One way ANOVA with Tukey's multiple comparison test *p<0.05.

Figure 6

Figure 6. Lacunar morphological analysis for the small lacunae 20-900 μm³ range.

Lacunae elongation, flatness and anisotropy analysis for (a, e, i) control, (b, f, j)

MGUS/SMM and (c, g, k) MM groups. Individual lacunae were assigned with eigenvalues

(EV1, EV2 and EV3) to then calculate lacuna elongation as EV2/EV1 (with lower values for

elongated and 1 for spherical) as (a-c) lacunar fraction (Lc.N/Lc.TN) and as (d) median of all

lacuna elongation values for each sample; lacuna flatness as EV3/EV2 (ranging from 0 for

flat to 1 for spherical) as (e-g) lacunar fraction (Lc.N/Lc.TN) and as (h) median of all lacuna

flatness values for each sample; and lacuna anisotropy as 1-EV3/EV1 (with smaller values

for isotropic/spherical and 1 for highest anisotropy) as (i-k) lacunar fraction (Lc.N/Lc.TN)

and as (l) median of all lacuna anisotropy values for each sample. Sample from the Jamshid

biopsy in black, all other control samples in grey. MGUS in blue, SMM in green, MM

samples with bone lytic lesion in red, MM samples without lytic lesions in orange. Error bars

indicate mean ± SD.

Tables

Table 1. Clinical data from MGUS patients from the University Hospital Würzburg

Parameters			
biopsy number	MGUS 1	MGUS 2	MGUS 3
age (years)	71	60	68
gender	f	m	f
immunoglobulin subtype	IgG lambda	IgG kappa	IgG kappa
r-ISS	not applicable	not applicable	not applicable
cytogenetic risk	not applicable	not applicable	not applicable
M-protein [g/L]	not detectable	not detectable	1,2
heavy chain [mg/dL, normal range]	1382 (610-1616)*	881 (610-1616)	507 (610-1616)
involved serum free light chain (sFLC) [mg/L, normal range]	23,89 (5,71-26,30)	10,75 (3,30-19,40)	215 (3,30-19,40)
ratio (involved / uninvolved sFLC)	0,86	1,02	5,44
bone marrow infiltration of CD138$^+$ cells [%]	<10	<10	<5
CT findings of osteolytic lesion	none	none	none
hemoglobin [g/dL]	12,9 (12-16)	14,4 (13,5-16,9)	12,7 (12-16)
creatinine [mg/dL]	0,63 (0-0,95)	1,06 (0-1,17)	6,69 (0-0,95)
cytogenetics**	no aberration	no aberration	no aberration
calcium [mmol/L]	2,2 (2,0-2,7)	2,5 (2,0-2,7)	2,3 (2,0-2,7)
alkaline phosphatase [U/L]	51 (35-105)	72 (35-105)	not available
inorganic phosphate [mmol/L]	1,09 (0,87-1,45)	1 (0,87-1,45)	1,85 (0,87-1,45)
bone anti-resorption treatment (duration)	Denosumab (four months)	no	no

749 * Values in brackets show the normal range for the parameters, respectively

750 ** Cytogenetic alterations by fluorescence in situ hybridization (FISH)

 Table 2. Clinical data from SMM patients from the University Hospital Würzburg

Parameters		
biopsy number	SMM 1	SMM 2
age (years)	46	70
gender	f	m
immunoglobulin subtype	IgA kappa	IgA lambda
r-ISS	II	I
cytogenetic risk	high risk	standard risk
M-protein [g/L]	not detectable	13,42
heavy chain [mg/dL, normal range]	1826 (88-410)	2826 (88-410)
involved serum free light chain (sFLC) [mg/L, normal range]	11,82 (3,30-19,40)	54,99 (5,71-26,3)
ratio (involved / uninvolved sFLC)	1,33	12,03
bone marrow infiltration of CD138$^+$ cells [%]	10-15	20-30
CT findings of osteolytic lesion	none	none
hemoglobin [g/dL]	12 (12-16)	13,2 (13,5-16,9)
creatinine [mg/dL]	0,78 (0-0,95)	0,91 (0-1,17)
cytogenetics	t4;14, gain of 1q21	del13q14
calcium [mmol/L]	2,2 (2,0-2,7)	2,4 (2,0-2,7)
alkaline phosphatase [U/L]	59 (35-105)	40 (35-105)
inorganic phosphate [mmol/L]	1,08 (0,87-1,45)	1,23 (0,87-1,45)
bone anti-resorption treatment (duration)	not known	no

755 **Table 3. Clinical data from newly diagnosed MM patients from the University Hospital**

756 **Würzburg**

Parameters			
biopsy number	MM 1	MM 2	MM 3
age (years)	58	57	72
gender	m	m	f
immunoglobulin subtype	IgG kappa	kappa	IgG lambda
r-ISS	III	II	III
cytogenetic risk	high risk	standard risk	high risk
M-protein [g/L]	35,3	not detectable	20,6
heavy chain [mg/dL, normal range]	4765 (610-1616)	not available	3074 (610-1616)
involved serum free light chain (sFLC) [mg/L, normal range]	71,12 (3,30-19,40)	8260 (3,30-19,40)	1376 (5,71-26,3)
ratio (involved / uninvolved sFLC)	40,41	890,09	355,56
bone marrow infiltration of CD138$^+$ cells [%]	70	60-70	90
CT findings of osteolytic lesion	osteolytic lesion with extraosseous soft tissue mass in spine (T12), lytic lesion in pelvis, rib series fractures, medullary lesions in femora and humeri, reduced bone mineral density	disseminated osteolysis in spine, one large lesion in T9 with increased fracture risk, old vertebral body collapse in T7 and fracture of the fourth left rib, multiple small osteolyses in scapulae, ribs, sternum reduced bone mineral density	no osteolytic lesions medullary lesions in upper and lower limbs, spine, sternum; reduced bone mineral density
hemoglobin [g/dL]	10,8 (13,5-16,9)	10,7 (13,5-16,9)	10,2 (12-16)
creatinine [mg/dL]	0,83 (0-1,17)	2,3 (0-1,17)	0,72 (0-0,95)
cytogenetics	t14;16, gain of 1q21	t11;14	del 17p, 1q gain, del14q, del 4p, del 16q, del 5p
calcium [mmol/L]	2,3 (2,0-2,7)	2,9 (2,0-2,7)	2,5 (2,0-2,7)
alkaline phosphatase [U/L]	97 (35-105)	80 (35-105)	49 (35-105)
inorganic phosphate [mmol/L]	1,25 (0,87-1,45)	1,33 (0,87-1,45)	0,99 (0,87-1,45)

bone anti-resorption treatment (duration)	bisphosphonate (zoledronic acid) for one month	no	no

758 **Table 3 (cont). Clinical data from newly diagnosed MM patients from the University**

759 **Hospital Würzburg**

Parameters			
biopsy number	MM 4	MM 5	MM 6
age (years)	60	68	64
gender	m	f	f
immunoglobulin subtype	IgA lambda	IgG kappa	IgG kappa
r-ISS	II	II	II
cytogenetic risk	standard risk	standard risk	standard risk
M-protein [g/L]	32,6	4,5	7,4
heavy chain (mg/dL, normal range)	4000 (88-410)	1180 (610-1616)	1625 (610-1616)
involved serum free light chain (sFLC) [mg/L, normal range]	33,8 (5,71-26,3)	16,59 (3,30-19,40)	309,8 (3,30-19,40)
ratio (involved / uninvolved sFLC)	4,26	1,49	8,41
bone marrow infiltration of CD138$^+$ cells [%]	30	50	60
CT findings of osteolytic lesion	osteolytic lesion in pelvis; mild reduction in bone mineral density	disseminated osteolysis in skull, spine, fracture series in spine (T7, 8, 11; L1, 2, 4), reduced bone mineral density in spine	none
hemoglobin [g/dL]	14 (13,5-16,9)	10,1 (12-16)	12,8 (12-16)
creatinine [mg/dL]	0,96 (0-1,17)	1,02 (0-0,95)	0,91 (0-0,95)
cytogenetics	del 1p32, del13q14, gain of 1q21	trisomy 11	gain of 1q21
calcium [mmol/L]	2,4 (2,0-2,7)	2,5 (2,0-2,7)	2,4 (2,0-2,7)
alkaline phosphatase [U/L]	41 (35-105)	95 (35-105)	92 (35-105)
inorganic phosphate [mmol/L]	1,19 (0,87-1,45)	0,94 (0,87-1,45)	0,74 (0,87-1,45)
bone anti-resorption treatment (duration)	no	no	no

761 **Table 4. Control samples: Jamshidi bone biopsy from a patient at the University**

762 **Hospital Würzburg and samples from autopsies at the Ludwig Boltzmann-Institute of**

763 **Osteology, Vienna.**

Parameters				
biopsy number	control 1	control 2	control 3	control 4
type of biopsy	jamshidi	autopsy*	autopsy*	autopsy*
age (years)	69	64	57	63
gender	f	f	f	f
previous disease	myelodysplastic syndrome	not known	not known	not known

764 * Subset of an earlier cohort presented previously [8] and re-evaluated here

766 **Table 5. Nomenclature for osteocyte lacunar volume analysis**

Nomenclature	Abbreviation	Unit
Number of osteocyte lacunae	Lc. N	-
Total number osteocyte lacunae	Lc. TN	-
Lacunar volume	Lc. V	μm^3
Total lacunar volume	Lc. TV	μm^3
Trabecular bone volume	Tb. BV	μm^3

767
768

769 **Table 6: Nomenclature for osteocyte lacunar morphological analysis**

Parameter	Definition	Unit	Formula
Normalized lacunar volume frequency distribution	Number of lacunae volume divided by the trabecular bone total volume minus the lacuna total volume	$\#/\mu m^3$	$\dfrac{\Sigma\, Lc.N}{Tb.TV - Lc.TV}$
Lacunar volume cumulative distribution	Sorted sum of volume divided by total volume	-	
Microporosity	Total lacunar volume with respect to the total trabecular bone volume	-	$\dfrac{Lc.TV}{Tb.TV}$
Lacuna elongation	0 for elongated 1 for spherical	-	$\dfrac{EV2}{EV1}$
Lacuna flatness	0 for flat 1 for spherical	-	$\dfrac{EV3}{EV2}$
Lacuna anisotropy	0 for isotropic, spherical 1 for highly anisotropic	-	$1 - \dfrac{EV3}{EV1}$