The effect of transcranial direct current stimulation of the dorsolateral prefrontal cortex on behavioral and brain activity indices of visuospatial attention in intrinsic reward contexts

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Abstract

Studies have suggested that the asymmetry of frontal brain activity is linked to self-regulation, particularly with approach tendencies in comparison to avoidance tendencies. However, the specific brain mechanism is not clear. Our preregistered study aimed to address the limitations of previous correlational studies by employing an interventional method, specifically non-invasive brain stimulation, regarding the connection between frontal alpha asymmetry (FAA) and the behavioral and brain activity components related to approach tendencies, as observed in a visuospatial cueing (VSC) paradigm. A randomized controlled triple-blind design was used, and the experiment involved 65 participants. During the study, participants' EEG was recorded and they performed a VSC task before and after the sham/active tDCS intervention The task included neutral and intrinsic reward-associated (food) conditions. The tDCS intervention consisted of 2 mA current applied to the right frontal F4 (anode) site relative to the left frontal F3 (cathode) site. The results showed no evidence that tDCS had an impact on FAA. There was also no indication of tDCS affecting the behavioral manifestations of attentional bias or disengagement. Surprisingly, secondary analyses concerning event-related potentials revealed that tDCS enhanced both the Late Directing Attention Positivity and P1 effect in the reward context. These findings suggest that tDCS might heighten cue-induced approach tendencies in a reward context, but these effects did not translate into observable behavioral changes. The observed effects are consistent with a noradrenergic mechanism rather than asymmetry of brain activity.

Keywords: ERP, frontal alpha asymmetry, inhibitory control, self-regulation, transcranial direct current stimulation, visuospatial attention

Impact Statement

We employed anodal right and cathodal left transcranial direct current stimulation (tDCS) over the dorsolateral cortex, to reduce attentional bias towards intrinsic reward-associated (food) stimuli. The tDCS did not significantly affect frontal alpha asymmetry; however, it enhanced attentional orienting in the reward context. The observed effect of the stimulation cannot be explained by the asymmetry of frontal brain activity and is more consistent with a noradrenergic mechanism.

1. Introduction

Self-regulation has been defined as "the self's ability to control its own thoughts, emotions, and actions" (Baumeister et al., 1994), and its failure has been associated with several mental health problems, such as depressive disorders and addictive disorders (Heatherton & Wagner, 2011; Johnstone et al., 2007). Previous studies also indicated that self-regulatory dysfunction is the main cause of numerous contemporary problems like obesity and sexual infidelity (Heatherton & Wagner, 2011). One plausible neural correlate of self-regulation is frontal alpha asymmetry (FAA), which can also be a treatment target for relevant disorders. More specifically, FAA is considered to be driven (at least in part) by activity within the dorsolateral prefrontal cortex (dLPFC) and represents a relative measure of the difference in alpha power (8-13 Hz) between the left and right cortices (Smith et al., 2017). Since the amplitude within the alpha frequency band represents inactivity, lower frontal asymmetry scores (right minus left alpha) reflect relatively less left than right cortical activity (Harmon-Jones et al., 2010). This asymmetry in frontal cortical activity has been associated with the two antagonistic components of self-regulation: approach and avoidance (Amodio et al., 2008; M.J.F. Robinson, A.M. Fischer, A. Ahuja, 2016). In particular, cues signaling reward trigger approach motivation, which is represented by left-over-right frontal brain activity, while cues signaling threat activate inhibitory motivation that is represented by right-over-left frontal brain activity (Coan et al., 2006; Harmon-Jones et al., 2010; Kelley et al., 2017). Hence, these mechanisms allow individuals to deal with rewards and threats that arise in their environment. Interestingly, assumed manipulation of FAA via transcranial direct current stimulation (tDCS) has been suggested to affect approach relative to avoidance tendencies; however, it remains uncertain whether tDCS directly impacts frontal brain activity asymmetry, and whether any effects on approach tendencies are mediated by tDCS-induced changes in frontal brain activity. Furthermore, the specific components underlying approach tendencies and their potential susceptibility to tDCS effects have not been elucidated. The present study aimed to investigate and provide answers to these questions (Houben et al., 2014; Luijten et al., 2011; Volkow et al., 2017).

In the realm of visuospatial attention, attentional bias and disengagement are two crucial components (Posner et al., 1980). When an observer anticipates a target at a particular position in a visual scene, a top-down mechanism called attentional bias leads to an accelerated processing of the target at the attended location (Corbetta & Shulman, 2002). Conversely, attentional disengagement is a target-driven bottom-up mechanism. When the observer has to focus on a more important object at the unattended site, it simplifies the decoupling of attention from the attended location, which simply facilitates a reorientation of attention (Logemann et al., 2014). The VSC task is a computer task used to investigate how attention is oriented in response to visual cues, which indicate the potential location of targets, and targets themselves (Posner et al., 1980). The most important behavioral outcome is the difference in response times (RTs) for validly cued targets and invalidly cued targets, which is called "validity effect," and it

is thought to reflect both attentional bias and attentional disengagement (Clark et al., 1989).

To explore these mechanisms, previous studies combined the VSC Task with EEG and event-related potential (ERP) reflections of attention-related processes. When an event occurs, large groups of neurons are activated synchronously, resulting in postsynaptic potentials that can be detected by EEG at specific times when time-locked to the event (Kappenman & Luck, 2012). Therefore, EEG allows us to distinguish brain activity associated with the onset of attentional bias (cue-related activity) from brain activity related to the outcome of this bias (target-related activity). For attentional bias, the sequence of ERPs consists of the Early Directing Attention Negativity (EDAN) and the Late Directing Attention Positivity (LDAP) indices of parietal activity. It also includes the Anterior Directing Attention Negativity (ADAN) of frontal activity (Van Der Lubbe et al., 2006). The outcome of bias was identified as the modulation of target-induced parietal P1 and N1 peaks by validity. More specifically, P1 and N1 are increased for validly cued targets compared to invalidly cued targets (Mangun & Hillyard, 1991; Meinke et al., 2006). Similarly, attentional disengagement is thought to be reflected in the modulation of the Late Positive Deflection (LPD) (Mangun & Hillyard, 1991; Meinke et al., 2006) in the areas that drive inhibitory control, including the right inferior Frontal Gyrus (rIFG) and temporal parietal junction (Corbetta et al., 2008), and it is larger to invalidly cued targets than validly cued targets. In addition, there is a conceptual overlap between attentional disengagement and inhibition since it also plays a central role in a response that has to be suddenly stopped due to a change in task demands (Logan et al., 1984; H N A Logemann et al., 2017; Posner et al., 1980). Previous studies show that stop signals (assessed by the Stop Signal Task (SST)) evoke a positivity of approximately 300 ms Latency (P300) that is modulated by successful inhibition (Lansbergen et al., 2007). Hence, it was argued that the LDP consists of P300 (Mangun & Hillyard, 1991): It is also enhanced when a specific stimulus requires attentional disengagement.

However, these mechanisms are not thoroughly studied in the context of the FAA and self-regulation. An ideal way to investigate them is to directly manipulate the asymmetry of frontal brain activity and to assess its effects on these ERPs and behavioral outcomes. To achieve this, we utilized tDCS. tDCS delivers low-level electrical currents through the scalp to change cortical activity in expected regions of the brain (Schestatsky et al., 2013). Results of a recent study suggest that tDCS over DLPFC affects self-regulation (Kekic et al., 2017).

To the best of our knowledge, prior studies have not taken into account the impact of tDCS on the functional asymmetry of the brain to determine whether the effects of tDCS are linked to frontal brain activity asymmetry. In this present study, we put forward the hypothesis that a tDCS intervention would lead to an elevation in right frontal brain activity compared to the left hemisphere. Additionally, we anticipated that active tDCS would decrease attentional bias, as indicated by behavioral and ERP measures, in the

reward context compared to the neutral context, while simultaneously enhancing attentional disengagement.

2. Methods

2.1. Participants

The rationale for the sample size was based on a within-subject pilot study (n = 10), where we estimated the effect size of tDCS concerning FAA as the primary measure. Specifically, using G*Power (Faul et al., 2007, 2009) with a defined power of 80 percent, alpha at .05, and an estimated FAA test-retest correlation of 0.6, we determined that a sample size of 30 in the active intervention group would allow us to detect an effect of f >0.237 or ηp2 > 0.053. Eligible participants were required to be at least 18 years old and had no psychological or psychiatric disorders, frequent headaches or migraines, metallic implants, epilepsy, significant head trauma in the past, recent head trauma, pacemaker, chronic skin conditions, current drug use, or low command of English. During the main study, some participants withdrew due to various reasons, such as boredom and fatigue. Consequently, a total of 65 adults (46 females) aged 18 to 58 ($M_{(age)}$ = 23.93; $SD_{(age)}$ = 6.08) were recruited through social media ads and university courses. Among them, fifty-seven were right-handed. All of the participants had at least a B1 level in English, based on Common European Framework of Reference for Languages - Self-assessment Grid (*Common European Framework of Reference for Languages: Learning, Teaching, Assessment*, 2001). These standard demographic questions were implemented in Psytoolkit (Stoet, 2010, 2017). Before participating, all individuals provided written informed consent. Each participant received either a voucher or course credit for participation. The study received approval from the Research Ethics Committee at Eötvös Loránd University and was conducted following the principles of the Declaration of Helsinki and its later amendments.

2.2. Visuospatial cueing task (VSC)

The VSC task was presented using OpenSesame (Mathôt et al., 2012). It was an adapted version from the original (Posner et al., 1980) and included an intrinsic reward condition based on previous research (Houben et al., 2014; Tsegaye et al., 2022) in addition to the neutral condition. Figure 1A illustrates the details of the task. Trials were randomized, and the condition order (neutral/reward) was counterbalanced across the participants. Only the first keyboard response to a target was logged for each trial. There were four main blocks (two for each condition) with a short practice block at the beginning of the task, and it took approximately 45 minutes in total. Participants were seated approximately 65 cm from the screen. The task began with clear instructions and verbal explanations when needed. Throughout the task, participants were instructed to keep their eyes fixed on the center of the screen. First, a fixation dot was presented for 2000 ms. Subsequently, a central cue (width: 100 (2.5°), height: 100 (2.5°)) was presented for 400 ms. The cue indicated to which side of the screen the participant had

to direct their attention. In the case of neutral cues, the cues did not indicate either the right or left side of the screen. Following that, a target was presented at either the left or right visual hemifield, which could be non-cued (presented after the neutral cue), valid (congruent with the location as indicated by the cue), or invalid (incongruent with the location indicated by the cue). The target was bar-shaped and could be either short (width: 200 (5.1°), height: 320 (8.1°)) or long (width: 200 (5.1°), height: 400 (10.2°)). The required response depended on the height of the bar, and stimulus-response assignments were counterbalanced across the participants. The intertrial interval was set to 3100 ms. The neutral and reward contexts differed in terms of the targets. Targets in the neutral condition consisted of solid grey bar-shaped targets. In the intrinsic reward condition, the bar-shaped targets represented palatable food images, such as chips, chocolate, cookies, and cashew nuts. These images are easy to recognize and are high in fat and sugar. Attentional bias was computed by subtracting the mean RT to valid targets from non-cued targets. A larger value indicates a stronger attentional bias. Attentional disengagement was computed by subtracting the RT to non-cued targets from invalidly cued targets. A larger value indicates lower attentional disengagement.

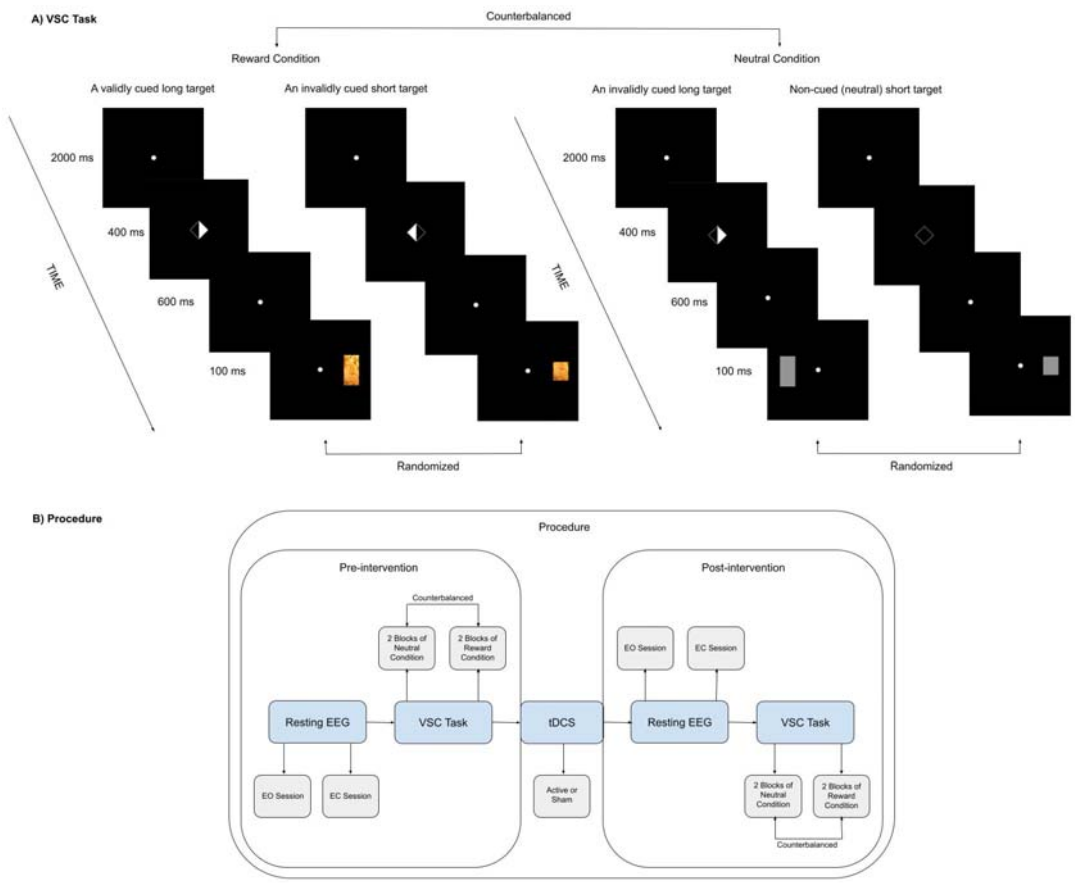

Figure 1. A) This figure illustrates four example trials in the VSC task. Depending on the counterbalanced order, participants began the VSC Task in either the neutral or reward condition. The first two trials (on the left) display a validly cued long target and an invalidly cued short in the reward condition, respectively. The last two trials (on the right) represent the

neutral condition. The last trial depicts a non-cued trial in which there is no cue indicating the potential location of a target and a short neutral target is displayed on the right hemifield. The target sizes overall and the target types in the reward condition (i.e., chocolate, cookies, nuts, and cashews) were randomized. B) The procedure begins with collecting pre-intervention resting state EEG data. It was collected in two sessions, one with 5 minutes of eyes open (EO) and another with 5 minutes of eyes closed (EC) conditions. Subsequently, participants performed the VSC task. Each participant received both the neutral and reward conditions in a counterbalanced order. Following that, either active or sham tDCS was administered. For further details regarding the intervention, please see Figure 2. After the tDCS intervention, we repeated the same procedure for the post-modulation assessment, which included the resting-state EEG and the VSC Task.

2.3. EEG recording

Scalp voltages were recorded using the NeXus-32 from Mind Media (*Nexus-32*, n.d.), employing a 21-channel cap Ag/AgCl electrodes placed according to the 10-20 system. The sampling frequency was 512 Hz, and activity was referenced to linked-ears. The horizontal electrooculography (HEOG) was recorded bipolarly from the outer canthi of both eyes, and the vertical EOG (VEOG) was recorded supra-relative to infra-orbital. EEG was recorded continuously except during tDCS application.

2.4. Frontal alpha asymmetry (FAA)

Frontal alpha asymmetry scores were calculated based on resting EEG states collected during 5 minutes of eyes open (EO) and 5 minutes of eyes closed (EC) sessions before and after the intervention. The EEG data was processed using BrainVision Analyzer 2 (www.brainproducts.com). Congruent with previous reports (Smith et al., 2017), FAA was calculated as follows. First, we applied a high-pass filter of 0.5 Hz, a low-pass filter of 40 Hz, and a 50 Hz notch filter. Then, we excluded the initial and final 10 seconds of each approximate 5-minute segment to account for potential artifacts. These segments were further divided into 2-second epochs. The epochs of the EO condition were corrected for ocular artifacts based on VEOG and HEOG electrodes using independent component analysis (ICA). The segments were baseline corrected using the -100 – 0 ms interval and whole-segment baseline corrected. Epochs containing any remaining artifacts (based on 75 µV max amplitude +/- relative to baseline criterion) were discarded, and Power Spectral Density (PSD) was calculated using Fast Fourier Transform FFT with a 10% Hanning window. Afterwards, the epochs were averaged and mean activity in the alpha frequency band (8-13 Hz) was calculated, and values were exported for the relevant electrodes. Alpha power was corrected for skew via natural log transform (Smith et al., 2017) using SPSS 22 (IBM Corporation, n.d.). Lastly, frontal asymmetry was calculated by subtracting the mean of log-transformed alpha at lateral left electrode sites from right electrode sites (F4-F3 and F8-F7). Thus, a higher FAA value reflects higher left frontal activity (i.e., lower left frontal alpha power).

2.5. Event-related potentials (ERPs)

EEG data were filtered (offline) using a low pass filter of 30 Hz, a high pass filter of 0.1592, and a notch filter of 50 Hz. Data were segmented into epochs ranging from -100 ms to 2300 ms cue-locked and from -100 to 1000 ms target-locked. Epochs were corrected for blinks (VEOG) using the Gratton et al., (Gratton et al., 1983) algorithm. Segments with evidence of horizontal eye movement higher than 60 µV were rejected (Van Der Lubbe et al., 2006). Subsequently, epochs were baseline-corrected with the baseline set at -100 to 0 ms. The cue-locked ERPs indicated previously were calculated in accordance with van der Lubbe et al. (Van Der Lubbe et al., 2006). The activity at ipsilateral electrodes was subtracted from the activity at contralateral electrodes relative to the cue direction for each participant. Based on van der Lubbe et al. (Van Der Lubbe et al., 2006), the EDAN and LDAP were quantified in the 240-280 ms and 560-640 ms time window at electrode pairs P3/P4 and T3/T4 respectively while the ADAN was quantified in the 400-480 ms at electrode pair F7/F8. However, after visual inspection of grand average waveforms, the latency of the 240-280 ms time window for the EDAN was adjusted to 190-250 ms while the ADAN time window 400-480 ms was adjusted to 320-400 ms. Based on Mangun and Hillyard (Mangun & Hillyard, 1991), the P1 and N1 were analyzed at parietal electrodes P3 and P4 and quantified as the mean amplitude in time windows 100-137 ms and 141-188 ms, respectively while the LPD was quantified as the mean amplitude in 229-299 ms time window at Cz electrode (Mangun & Hillyard, 1991). The P1, N1, and LPD *effects* were computed by subtracting the mean activity within the aforementioned time windows relative to invalidly cued target onset from the activity relative to validly cued target onset.

2.6. Transcranial direct current stimulation (tDCS)

Brain modulation aimed to increase the activity of the right relative to the left dorsolateral prefrontal cortex. Direct electrical current was transmitted using a pair of saline-soaked, circular, sponge electrodes (25 cm^2) and delivered via STARSTIM-8, Neuroelectrics (www.neuroelectrics.com). The anode was placed on the right dLPFC (F4), while the cathode was placed on the left DLPC (F3), based on the 10–20 system. A constant current of 2 mA was applied for 20 minutes (Kelley et al., 2017) (Fig.2) unless it was a sham condition. In the sham condition, the same electrical current was only briefly applied at the beginning of the session to generate a similar experience. The employed tDCS procedures have been demonstrated to be safe in healthy participants (Iyer et al., 2005).

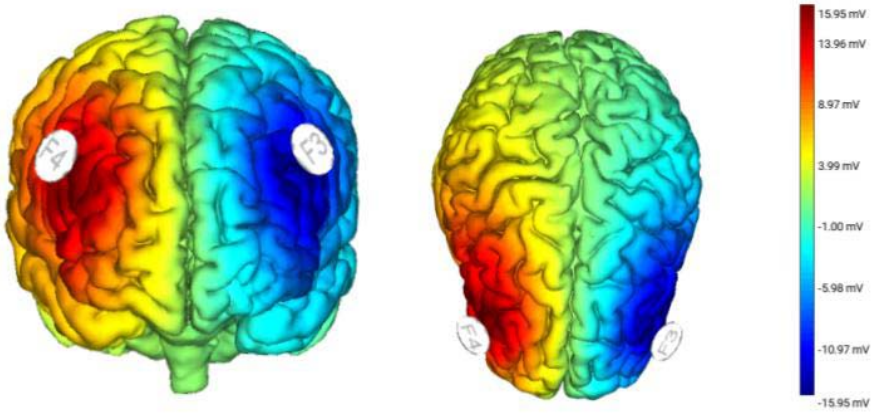

Figure 2. This figure shows the placement of the tDCS electrodes and measured electric fields from the front and top, respectively. A constant current of 2 mA was applied via two circular sponge electrodes (25 cm^2), placed over positions F4 (anode) and F3 (cathode) with saline solution. The maximal electric field strength was 15.95 µV for the anodal electrode.

2.7. Procedure

We employed a randomized, triple-blind, sham-controlled design. We considered within-subject factors, including time (pre-/post-intervention) and condition (neutral/reward), as well as a between-subject factor, which was the group (active/sham tDCS). We preregistered our detailed research plan on Open Science Framework (https://osf.io/5hvpw?view_only=b528cd416ff047e8be789bc4da284f36). When a participant arrived at our laboratory, they read the information letter, checked the exclusion criteria, and signed the informed consent form. Subsequently, they were seated in a comfortable chair in a dimly lit testing room for the placement of EEG electrodes on the scalp. After placing the electrodes, we collected resting EEG data, recording it for a total of 10 minutes, with blocks of five minutes for both EO and EC sessions. Following the resting EEG recording, participants completed the questions. Subsequently, they proceeded to the first part of the VSC Task before the tDCS intervention. Subsequently, they were randomly assigned to receive either active or sham tDCS. After the tDCS intervention, we conducted the same procedure again for the post-modulation assessment, including the resting-state EEG and the VSC Task. Please consider Figure 1B for more details. The pre-/post-assessments and the intervention all took place on the same day, lasting approximately five hours.

2.8. Statistical analyses

The statistical analyses were conducted using SPSS 22 (IBM Corporation, n.d.) and R (*R Software: A Tool Analysing Experimental Data*, 2016). After the calculations of the main variables, participants with missing values and outliers exceeding 3 standard deviations (SD) from the mean were excluded in case of evident erroneous data. Then, we used repeated measures ANOVA (2x2x2) to test the hypotheses. The electrophysiological

variables under investigation included FAA (EO/EC), ADAN, EDAN, LDAP, N1 *effect,* P1 *effect*, and LPD *effect*, as well as the behavioral indices of attentional bias and disengagement. For all analyses, the significance level was set at 0.05. Secondary analyses were performed on the behavioral and ERP indices of attentional processes, excluding participants who showed an absent validity effect at baseline in the VSC task. Additionally, exploratory analyses were conducted to explore the effects of time and group in the reward condition.

3. Results

3.1. Did the tDCS have an impact on frontal alpha asymmetry?

To test whether the tDCS intervention affected FAA, we conducted a repeated measures of ANOVA with the within-subjects factor of time (pre-/post-intervention) and the between-subject factor of group (active/sham tDCS) on FAA scores. The analysis showed that there is no significant interaction of time and group factors on FAA. Table 1 shows the details of the results.

Table 1. Results of FAA Models

Variables	Df	F	P	η_p^2
FAA F4-F3 (EO) (N = 59)				
Group	1	3.64	0.058	0.030
Time	1	0.39	0.530	0.003
Group x Time	1	0.28	0.594	0.002
Error	114			
FAA F4-F3 (EC) (N = 59)				
Group	1	1.22	0.271	0.010
Time	1	1.27	0.261	0.010
Group x Time	1	0.49	0.484	0.004
Error	114			
FAA F8-F7 (EO) (N = 62)				
Group	1	0.00	0.951	<0.001
Time	1	0.00	0.933	<0.001
Group x Time	1	0.29	0.588	0.002
Error	120			
FAA F8-F7 (EC) (N =59)				
Group	1	0.03	0.849	<0.001
Time	1	3.58	0.060	0.030
Group x Time	1	0.08	0.769	<0.001
Error	114			

Note: Participants with missing values and erroneous data were excluded from the analyses.

3.2. Did the tDCS affect the behavioral indices of visuospatial attention?

We conducted a series of repeated measures ANOVA with the within-subject factors of time (pre-/post-intervention) and condition (neutral/reward), as well as the between-subject factor of group (active/sham tDCS). The statistical results are provided in Table 2. Although there was a significant main effect of condition on attentional disengagement, $F(1, 232) = 8.59$, $p = 0.003$, $\eta_p^2 = 0.035$, its interaction with time and group factors was not significant $F(1, 232) = 0.01$, $p = 0.909$, $\eta_p^2 = <0.001$. The direction of the relationship between attentional disengagement and condition was illustrated in Figure 3. The figure revealed reduced attentional disengagement (increased attentional engagement) in the reward condition compared to the neutral condition.

Table 2. Results of attentional bias and attentional disengagement models

Variables	Df	F	P	η_p^2
Attentional Bias (N = 60)				
Time	1	0.01	0.917	<0.001
Condition	1	2.60	0.108	0.011
Group	1	2.05	0.153	0.008
Time x Condition	1	0.18	0.670	<0.001
Time x Group	1	1.22	0.270	0.005
Condition x Group	1	0.03	0.851	<0.001
Time x Condition x Group	1	0.11	0.730	<0.001
Error	232			
Attentional Disengagement (N = 60)				
Time	1	0.42	0.517	0.001
Condition	1	8.59	0.003*	0.035
Group	1	2.05	0.153	0.008
Time x Condition	1	2.44	0.119	0.010
Time x Group	1	0.67	0.413	0.002
Condition x Group	1	0.17	0.677	<0.001
Time x Condition x Group	1	0.01	0.909	<0.001
Error	232			

Note: Participants with missing values and erroneous data were excluded from the analyses.

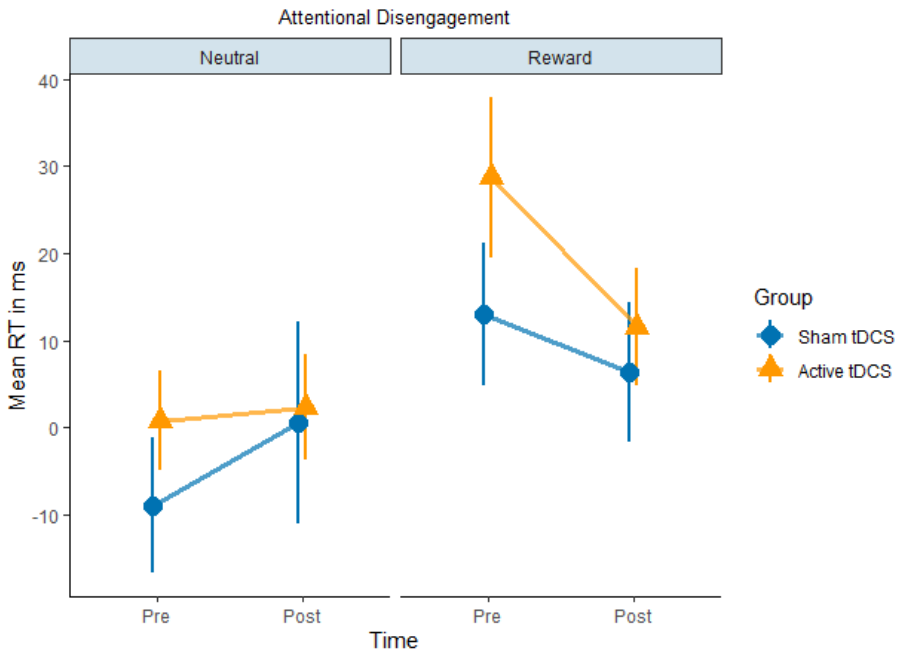

Figure 3. This figure shows the mean RTs of attentional disengagement based on time (pre-/post-intervention), condition (neutral/reward), and group (sham/active tDCS) factors. It depicts reduced attentional disengagement (increased attentional engagement) in the reward condition compared to the neutral condition. Please note that attentional disengagement was calculated by subtracting the mean RT to non-cued targets from invalidly cued targets. Therefore, a greater value indicates lower attentional disengagement.

3.3. Did the tDCS affect cue-locked event-related potentials?

A series of repeated measures ANOVA was conducted on each cue-locked ERP. The within-subject factors included time (pre-/post-intervention) and condition (neutral/reward), while the between-subject factor was group (active/sham tDCS). The results concerning the EDAN, ADAN, and LDAP can be observed in Figures 4, 5, and 6, respectively. For detailed inferential statistics, refer to Table 3. We found that the effect of time, condition, and group interactions on LDAP showed a trend towards significance, $F(1, 56) = 2.98$, $p = 0.090$, $\eta_p^2 = 0.051$.

Table 3. Results of cue-locked ERP models

Variables	Df	F	p	η_p^2
EDAN at 190-250 ms. (P4/P3) (N = 58)				
Time	1	2.13	0.149	0.037
Condition	1	0.71	0.402	0.013
Group	1	0.71	0.401	0.013
Time x Condition	1	0.69	0.408	0.012
Time x Group	1	3.09	0.084	0.052
Condition x Group	1	<0.01	0.991	<0.001
Time x Condition x Group	1	0.28	0.597	0.005
Error	56			
ADAN at 320-400 ms. (F8/F7) (N = 58)				
Time	1	0.92	0.762	0.002
Condition	1	0.11	0.738	0.002
Group	1	0.07	0.784	0.001
Time x Condition	1	1.57	0.215	0.027
Time x Group	1	0.20	0.656	0.004
Condition x Group	1	0.86	0.356	0.015
Time x Condition x Group	1	2.23	0.141	0.038
Error	56			
LDAP at 560-640 ms. (T4/T3) (N = 58)				
Time	1	0.11	0.733	0.002
Condition	1	0.01	0.896	<0.001
Group	1	0.02	0.874	<0.001
Time x Condition	1	<0.01	0.958	<0.001
Time x Group	1	0.01	0.899	<0.001
Condition x Group	1	<0.01	0.923	<0.001
Time x Condition x Group	1	2.98	0.090	0.051
Error	56			

Note: Participants with missing values and erroneous data were excluded from the analyses.

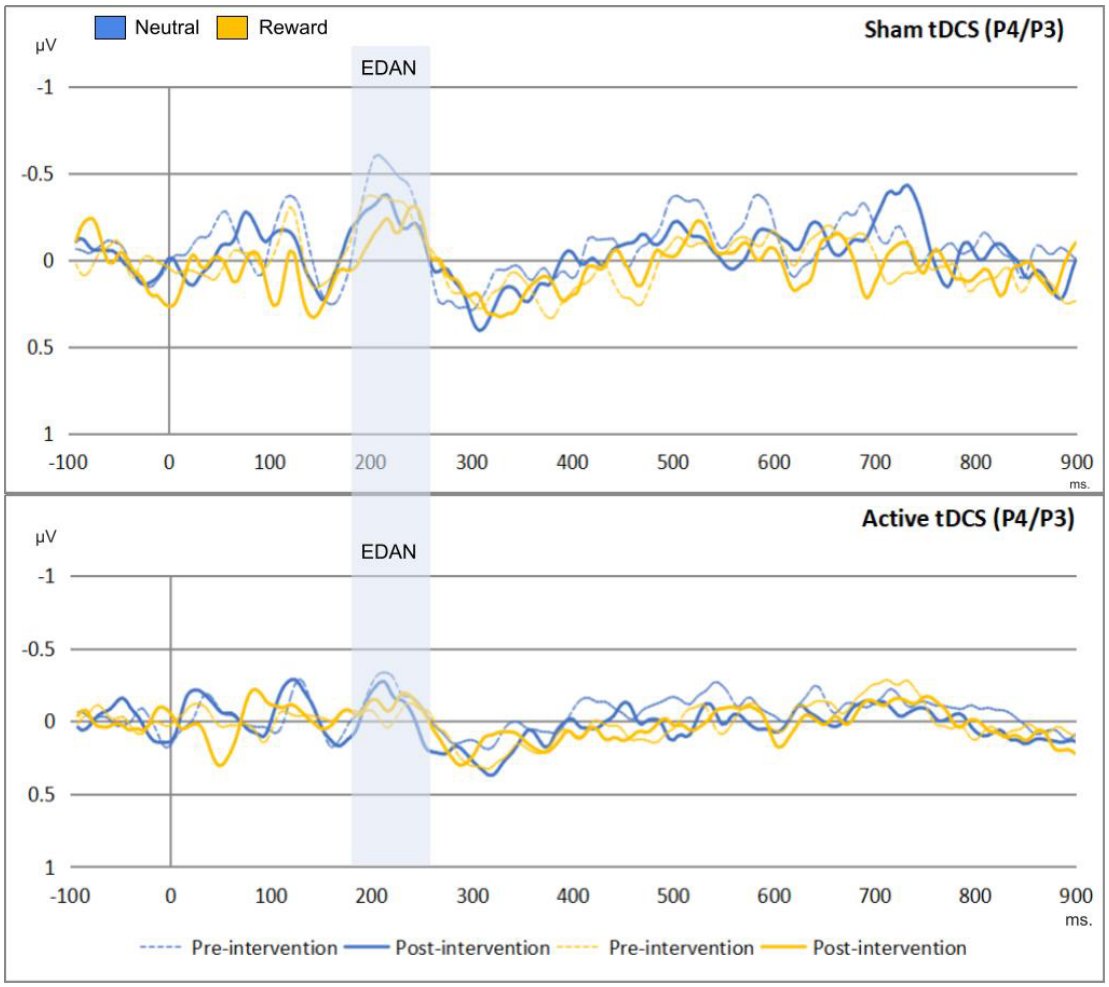

Figure 4. This figure shows the effects of time, condition, and group on the EDAN (190-250 ms). The x-axes represent the time in milliseconds while y-axes represents the EDAN scores in microvolts. Based on the depiction, the EDAN was replicated in the study regardless of time, condition, and group effects.

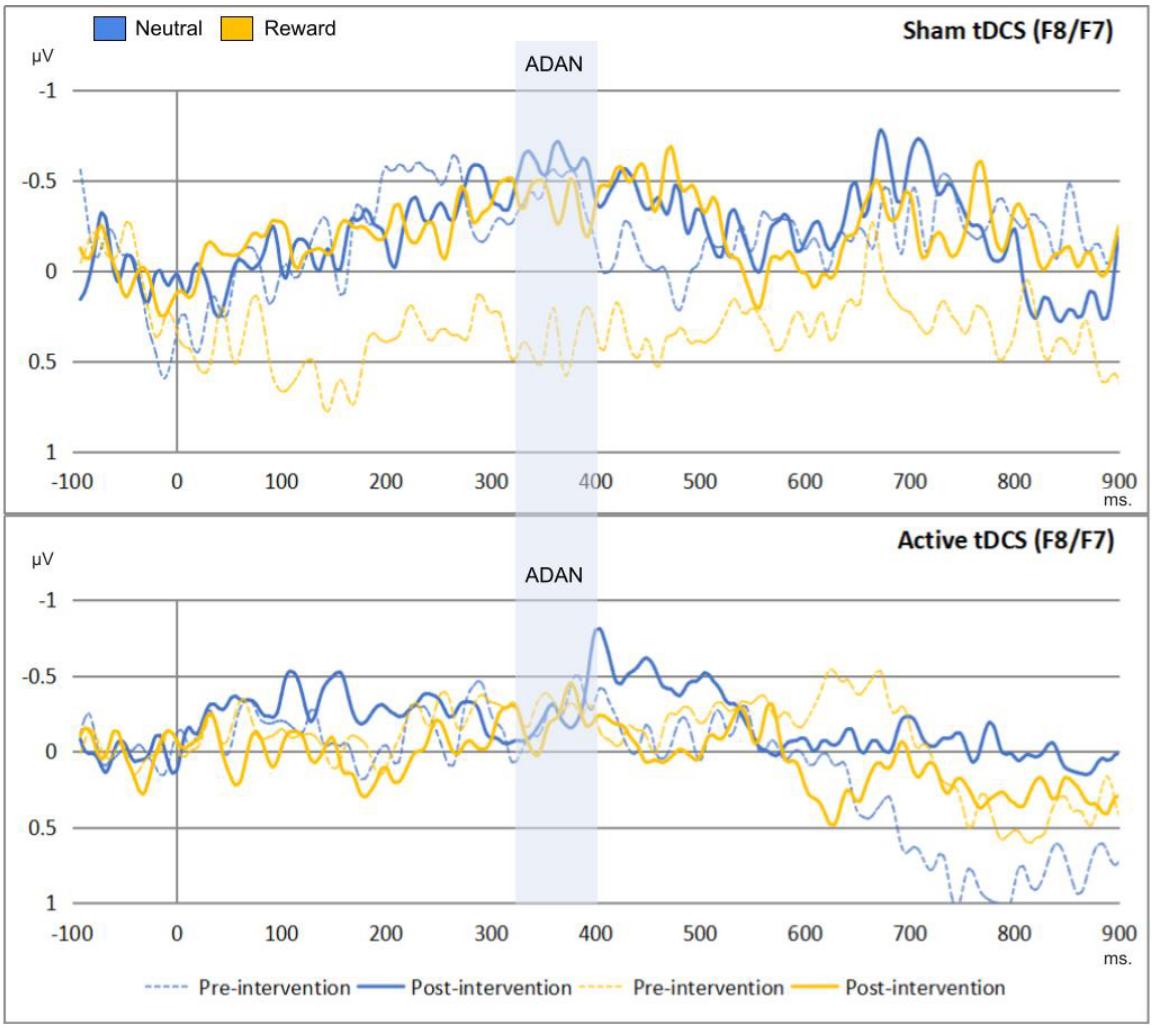

Figure 5. This figure shows the effects of time, condition, and group on the ADAN (190-250 ms). The x-axes represent the time in milliseconds while y-axes represents the EDAN scores in microvolts. Based on the illustration, the ADAN was replicated in the study even though there were no significant effects of time, condition, and group factors.

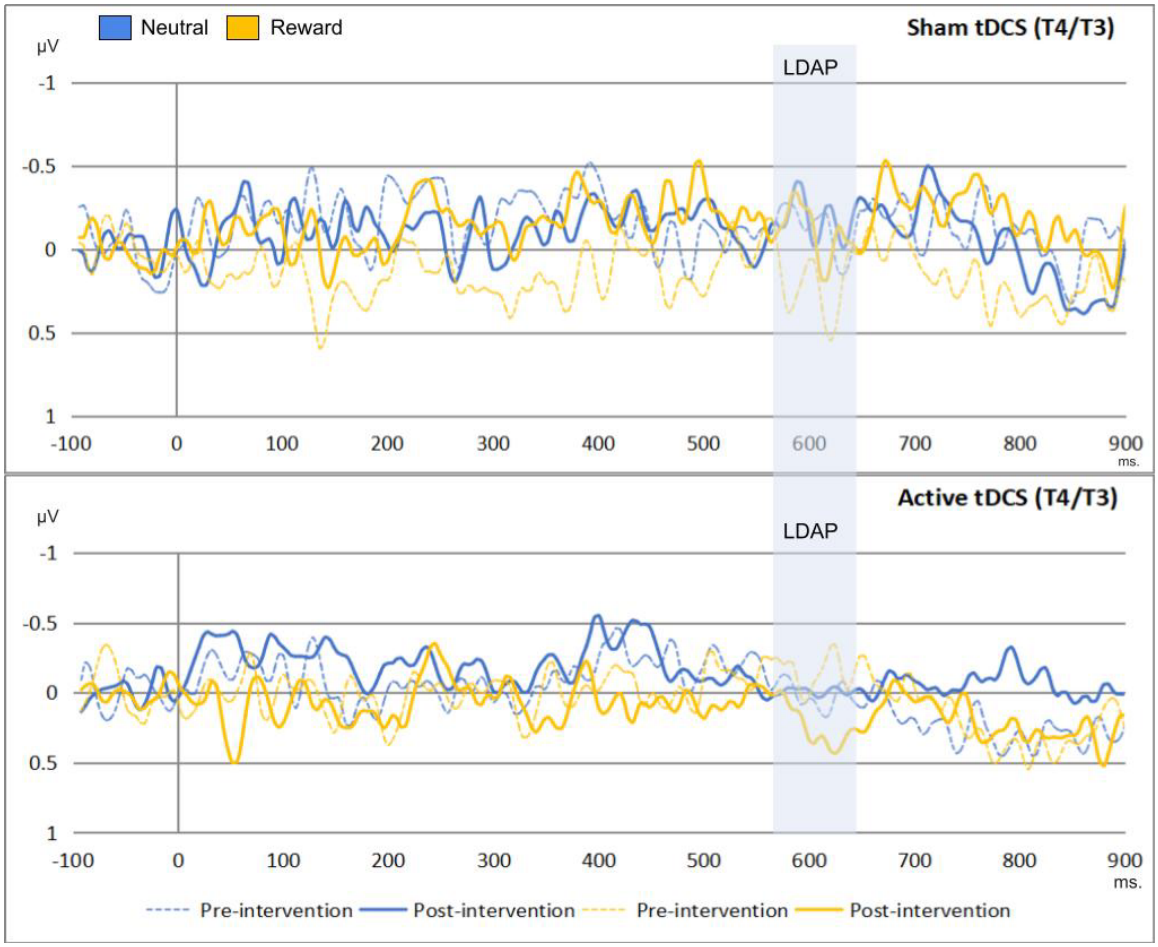

Figure 6. This figure shows the effects of time, condition, and group on the LDAP (560-640 ms). The x-axes represent the time in milliseconds while y-axes represents the EDAN scores in microvolts. Based on the depiction, the LDAP was replicated in the study.

3.4. Did the tDCS affect target-locked event-related potentials?

We conducted a series of repeated measures ANOVA to assess whether the tDCS intervention influenced the target-locked ERPs. The within-subject factors for the models were time (pre-/post-intervention) and condition (neutral/reward), while the between-subject factor was group (active/sham tDCS). We found that there was no significant effect of time, condition, and group interactions on target-locked ERPs as shown in Table 4, Table 5, and Table 6 for the P1 *effect*, N1 *effect*, and LPD *effect*, respectively. These results are also illustrated in Figure 7 and Figure 8. Similar to previous explorations, the P1 *effect* was not identified (Logemann et al., 2014).

Table 4: Results of P1 models

Variables	Df	F	p	η_p^2
P1 at 100-137 ms. (P3) (N = 55)				
Intercept		1.25	0.269	0.023
Time	1	1.85	0.179	0.034
Condition	1	0.05	0.818	0.001
Group	1	0.90	0.347	0.017
Time x Condition	1	1.09	0.084	0.055
Time x Group	1	0.19	0.662	0.004
Condition x Group	1	0.82	0.368	0.015
Time x Condition x Group	1	0.37	0.545	0.007
Error	53			
P1 at 100-137 ms. (P4) (N = 55)				
Intercept		0.79	0.375	0.015
Time	1	2.60	0.113	0.047
Condition	1	0.25	0.257	0.024
Group	1	1.37	0.246	0.025
Time x Condition	1	2.40	0.127	0.043
Time x Group	1	1.31	0.257	0.024
Condition x Group	1	3.88	0.054	0.068
Time x Condition x Group	1	0.01	0.896	<0.001
Error	53			

Note: Participants with missing values and erroneous data were excluded from the analyses.

Table 5: Results of N1 Models

Variables	Df	F	p	η_p^2
N1 at 141-188 ms. (P3) (N = 55)				
Intercept	1	2.96	0.091	0.053
Time	1	2.25	0.140	0.041
Condition	1	0.18	0.666	0.004
Group	1	1.20	0.277	0.022
Time x Condition	1	1.28	0.262	0.024
Time x Group	1	<0.01	0.994	<0.001
Condition x Group	1	<0.01	0.936	<0.001
Time x Condition x Group	1	0.78	0.379	0.015
Error	53			
N1 at 141-188 ms. (P4) (N = 55)				
Intercept	1	8.59	0.005*	0.140
Time	1	1.42	0.238	0.026
Condition	1	<0.01	0.940	<0.001
Group	1	0.44	0.509	0.008
Time x Condition	1	1.51	0.224	0.028

Time x Group	1	0.99	0.324	0.018
Condition x Group	1	0.15	0.695	0.003
Time x Condition x Group	1	0.15	0.694	0.003
Error	53			

Note: Participants with missing values and erroneous data were excluded from the analyses.

Table 6: Results of the LPD model

Variables	Df	F	p	η_p^2
LPD at 229-299 ms. (Cz) (N = 55)				
Intercept	1	6.62	0.013*	0.111
Time	1	3.37	0.072	0.060
Condition	1	0.34	0.559	0.006
Group	1	1.26	0.267	0.023
Time x Condition	1	2.86	0.097	0.051
Time x Group	1	0.11	0.734	0.002
Condition x Group	1	1.66	0.202	0.030
Time x Condition x Group	1	0.14	0.703	0.003
Error	53			

Note: Participants with missing values and erroneous data were excluded from the analyses.

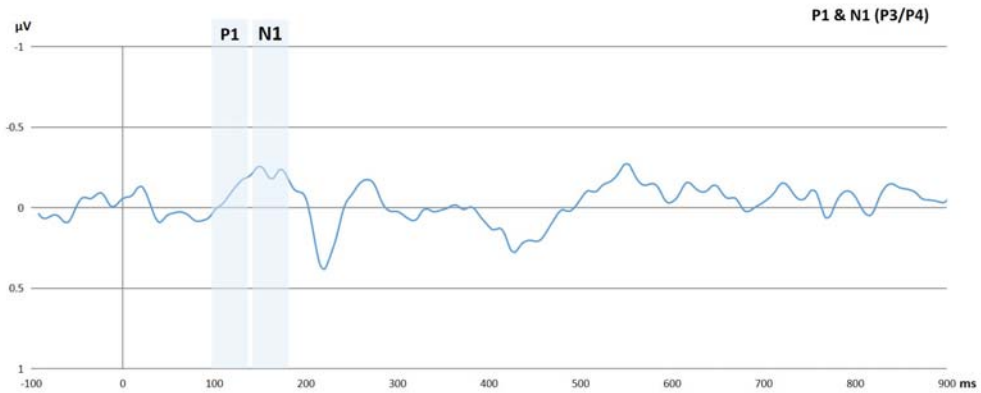

Figure 7. The figure shows the P1 *effect* and N1 *effect*. The x-axis represents the time in milliseconds while y-axis represents the P1 *effect* and N1 *effect* scores in microvolts. The P1 effect was calculated by subtracting the P1 to invalid trials from the P1 to valid trials. Similarly, the N1 was calculated by subtracting the N1 to invalid trials from the N1 to valid trials.

Figure 8. The figure shows the LPD *effect*. The x-axis represents the time in milliseconds while y-axis represents the LPD *effect* scores in microvolts. The LPD *effect* was calculated by subtracting the LPD to invalid trials from the LPD to valid trials. Therefore, the negative peak represents an enhanced LPD for invalid trials relative to valid trials as well as a reduced LPD for valid trials relative to invalid trials.

3.5. Exploratory analyses

In line with a previously reported approach (Thiel & Fink, 2008), secondary analyses were conducted with individuals who showed a validity effect at baseline in both neutral and reward conditions. As stated previously, the validity effect was calculated based on higher RTs in invalid trials than in valid trials (invalid trials > valid trials). Following analyses were conducted based on this selected sample.

Similar to the previous results, the main effect of condition on attentional disengagement was significant, $F(1, 128) = 4.86$, $p = 0.029$, $\eta_p^2 = 0.034$. Indeed, secondary analyses based on the validity effect did not yield any additional information regarding the behavioral indices of visuospatial attention. Please see Table 7 in the supplementary file for further information.

We also tested the effect of time and group interactions on electrophysiological indices of visuospatial attention in the neutral and reward conditions. Both the LDAP and P1 *effect* were enhanced in the active tDCS group relative to the sham tDCS group in the reward context, $F(1, 30) = 6.70$, $p = 0.015$, $\eta_p^2 = 0.183$ and $F(1, 30) = 6.30$, $p = 0.018$, $\eta_p^2 = 0.174$, respectively. They can also be seen in Figure 9 and 10, respectively. Please also consider Table 10 and Table 14 in the supplementary file for more information.

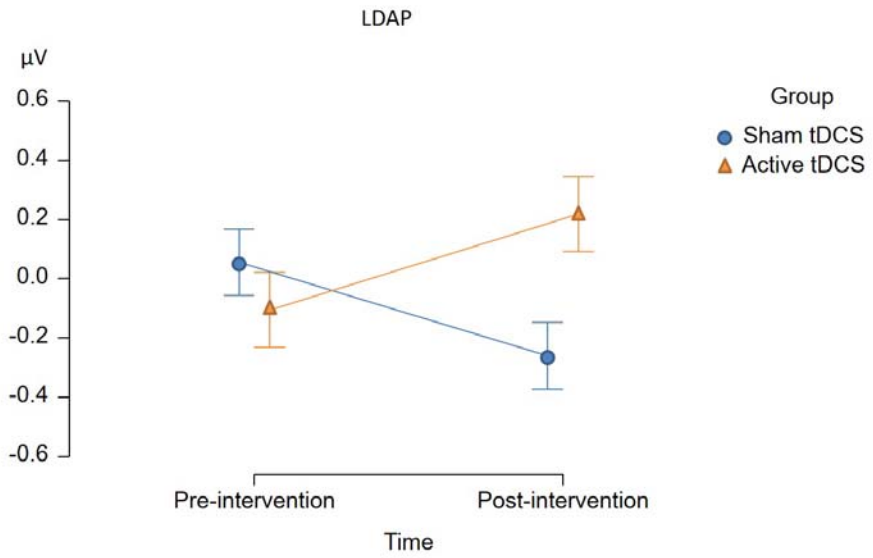

Figure 9. The figure shows the exact effect of time and group interactions on the LDAP in the reward context. The x-axis represents the time factor while y-axis represents the LDAP in microvolts.

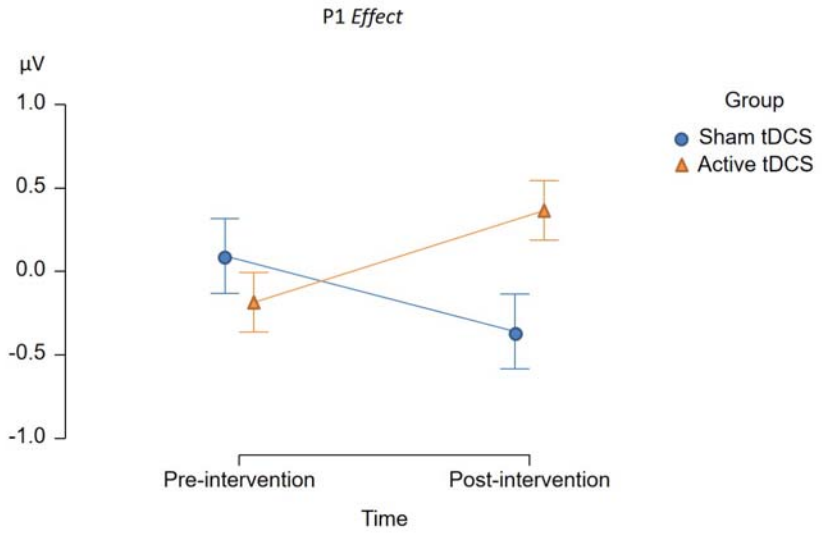

Figure 10. The figure shows the exact effect of time and group interactions on the P1 effect in the reward context. The x-axis represents the time factor while y-axis represents the P1 effect in microvolts.

4. Discussion

The present study investigated the effect of tDCS on FAA as a potential neurophysiological index of self-regulation, as well as on behavioral and brain activity indices of visuospatial attention under the influence of intrinsic reward-related stimuli, specifically palatable food images. The results revealed no significant effect of tDCS on FAA. On the other hand, the exploratory analyses regarding the electrophysiological indices of visuospatial attention demonstrated a statistically significant enhancement of attentional orienting towards food stimuli in the active tDCS group compared to the sham tDCS group. Nevertheless, the effect of tDCS did not translate into observable behavioral changes. We only observed a statistically significant main effect of condition on the RTs, indicating reduced attentional disengagement (increased attentional engagement) in the reward condition compared to the neutral condition.

Previous studies suggested that tDCS may affect the asymmetry of frontal brain activity (Kekic et al., 2017). Despite their relevance, these measures are considered indirect. Importantly, to the best of our knowledge, prior studies have not thoroughly investigated whether tDCS actually affects the primary target, which is the asymmetry of frontal brain activity. Our results did not show any support for tDCS-induced shifts in the asymmetry of frontal brain activity, as indexed by FAA. Though contrary to our hypothesis, the lack of a significant effect may not be too surprising. The path of electric currents is complex, involving the electrodes, scalp, skull, meninges, and cerebrospinal fluid before reaching the brain. However, each brain has a unique anatomical structure, resulting in different magnitudes and directions of the electric field in each subject (Laakso et al., 2015; Opitz et al., 2015; Truong et al., 2013). Indeed, not only neuronal structure, such as skull thickness, sulcal depth, and gyral depth, can influence the electric field strength but also there may be "hotspots" that resist electrode positioning (Opitz et al., 2015). Especially when compared to motor cortical tDCS, frontal tDCS produces more variable electric fields (Laakso et al., 2016). This variability may lead to conflicting results in brain stimulation studies (Tremblay et al., 2014). Aside from the variations in individual brain anatomy, the effects of stimulation can also be influenced by factors such as electrode properties, including size and shape, and conductivities, such as gels and saline solutions (Saturnino et al., 2015). Therefore, these findings in the literature suggest that the lack of a significant effect of tDCS on FAA in our study may be attributed to the variability in individual brain structures, the influence of electrode positioning, and the diverse effects of tDCS montages and electrode properties on stimulation outcomes. Future studies should take into account and control for individual differences to ensure the validity and reliability of the findings.

Even though primary analyses did not reveal a significant effect of tDCS on attentional bias and disengagement at the behavioral level, the results indicated a potential effect of tDCS on the electrophysiological measure of attentional orienting, which was confirmed in our exploratory analyses. For these analyses, we employed the same approach as in

Thiel et al. (Thiel & Fink, 2008) and excluded participants who did not show evidence of cue-induced manipulation of attention. In the resulting sample, tDCS resulted in an enhanced cue-induced LDAP specifically in the reward context. This can be interpreted as a tDCS-induced enhancement of top-down attentional orienting to spatial locations associated with upcoming reward-associated stimuli. Surprisingly, this effect contradicts the hypothesized shift toward enhanced right versus left frontal activity in our study and previous studies. More specifically, previous research has reported that tDCS enhances inhibitory control (Kekic et al., 2017). The effect of tDCS on enhancing inhibitory control might arguably outweigh its impact on attentional bias and any potential associated response complicating inhibitory control. Therefore, the question arises as to which alternative mechanism fits the observed effect. Likewise, a study found positive effects on inhibitory control irrespective of the stimulation site, pointing towards a more general mechanism: Both anode right/cathode left and anode left/cathode right tDCS increased inhibitory control (Kekic et al., 2017). The answer to these questions can potentially be found in animal studies. Animal studies suggest that tDCS generates a subthreshold depolarization of neuronal membrane potential, leading to an increased likelihood of neuronal discharge and/or synaptic transmission (Monai et al., 2016; Monai & Hirase, 2016, 2017). It was reported that tDCS induces cerebral plasticity based on calcium (Ca2+) elevation of astrocytic origin in mice. This tDCS-induced Ca2+ elevation is blocked by noradrenergic neuron ablation. Together these imply that tDCS results in increased Noradrenaline (NA) release (Monai et al., 2016; Monai & Hirase, 2016, 2017). The question is whether enhanced attentional orienting and inhibitory control can be explained by increased noradrenergic neurotransmission. Previous studies in psychopharmacology lend support to this notion. In a study, noradrenergic challenge with Clonidine resulted in a reduction of attentional bias, as indexed by electrophysiology. Hence, inversely, facilitation of NA plausibly results in enhanced attentional bias, which aligns with the current observed results in the study (Logemann et al., 2014). On the other hand, another study on inhibitory control indicated that inhibitory activity (evidenced by the Stop P3) is reduced following attenuated NA neurotransmission (Logemann et al., 2013). Therefore, tDCS enhancement of NA would likely result in improved inhibitory control simultaneously.

Lastly, the only significant behavioral effect in the experiment was the main effect of condition on attentional disengagement. We unsurprisingly found that attentional disengagement was reduced in the reward condition compared to the neutral condition regardless of group. In the absence of a significant effect from tDCS, we can expect food stimuli to pose a challenge to attentional disengagement potentially. This finding is in line with similar studies reporting that food stimuli challenge inhibitory control (Houben et al., 2014; Jasinska et al., 2012).

Despite the valuable insights gained from this study, several limitations need to be addressed. First, as indicated previously, individual variations in brain anatomy might have contributed to the null effects. Besides, the effectiveness of tDCS is contingent on various factors including stimulation parameters (e.g., duration, intensity, electrode

placement). While the chosen intervention parameters were based on existing literature and rationale, other stimulation settings could have yielded different results. In the current study, the tDCS intervention was administered in a single session. Multiple sessions might produce different effects on frontal brain activity, potentially influencing the observed outcomes. Although FAA was investigated as a primary mediator, this study highlights that other neurobiological/neurochemical mechanisms, such as the noradrenergic system, may underlie the observed effects regarding attentional reorienting. However, the specific mechanisms were not directly explored in this study, leaving room for further investigation. Overall, while the study contributes important groundwork in this area, the identified limitations should be taken into consideration while interpreting the findings and for future research.

Conclusion

In conclusion, this preregistered study explored the relationship between frontal alpha asymmetry (FAA), approach tendencies, and transcranial direct current stimulation (tDCS) within a visuospatial cueing paradigm. While tDCS did not show significant effects on FAA or behavioral attentional processes, intriguing secondary findings suggest tDCS might enhance cue-induced approach tendencies in a reward context. However, these effects did not lead to observable behavioral changes. Our study highlights the potential involvement of the noradrenergic system in the effect of tDCS on attentional orienting to reward associated stimuli.

Data Availability Statement

All data and codes can be found on our online public repository.

Ethics Statement

The study received approval from the Research Ethics Committee at Eötvös Loránd University (project number: 2020/403) and was conducted following the principles of the Declaration of Helsinki and its later amendments.

Author Contributions

AMA: Conceptualization, Methodology, Formal Analysis, Investigation, Data Curation, Writing - Original Draft, Visualization, Project Administration. RC: Conceptualization, Methodology, Resources, Writing - Review & Editing, Supervision. DN: Conceptualization, Methodology, Resources, Writing - Review & Editing, Supervision. TN: Conceptualization, Methodology, Writing - Review & Editing, Supervision. ZD: Conceptualization, Methodology, Writing - Review & Editing, Supervision. AL: Conceptualization, Methodology, Formal Analysis, Resources, Data Curation, Writing - Review & Editing, Supervision, Funding acquisition.

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Conflict of Interest

The authors declare that the research was conducted in the absence of any commercial or financial relationships that could be construed as a potential conflict of interest.

References

Amodio, D. M., Master, S. L., Yee, C. M., & Taylor, S. E. (2008). Neurocognitive components of the behavioral inhibition and activation systems: Implications for theories of self-regulation. *Psychophysiology*, *45*(1), 11–19. https://doi.org/10.1111/j.1469-8986.2007.00609.x

Baumeister, R. F., Heatherton, T. F., & Tice, D. M. (1994). Losing control: How and why people fail at self-regulation. In *Losing control: How and why people fail at self-regulation*. Academic Press.

Clark, C. R., Geffen, G. M., & Geffen, L. B. (1989). Catecholamines and the covert orientation of attention in humans. In *Neuropsychologia* (Vol. 27, pp. 131–139). Elsevier Science. https://doi.org/10.1016/0028-3932(89)90166-8

Coan, J. A., Allen, J. J. B., & McKnight, P. E. (2006). A capability model of individual differences in frontal EEG asymmetry. *Biological Psychology*, *72*(2), 198–207. https://doi.org/10.1016/j.biopsycho.2005.10.003

Common European Framework of Reference for Languages: Learning, Teaching, Assessment. (2001). Cambridge University Press.

Corbetta, M., Patel, G., & Shulman, G. L. (2008). The reorienting system of the human brain: from environment to theory of mind. *Neuron*, *58*(3), 306–324. https://doi.org/10.1016/j.neuron.2008.04.017

Corbetta, M., & Shulman, G. L. (2002). Control of goal-directed and stimulus-driven attention in the brain. *Nature Reviews Neuroscience*, *3*(3), 201–215. https://doi.org/10.1038/nrn755

Faul, F., Erdfelder, E., Buchner, A., & Lang, A.-G. (2009). Statistical power analyses using G*Power 3.1: Tests for correlation and regression analyses. *Behavior Research Methods*, *41*(4), 1149–1160. https://doi.org/10.3758/BRM.41.4.1149

Faul, F., Erdfelder, E., Lang, A.-G., & Buchner, A. (2007). G*Power 3: A flexible statistical power analysis program for the social, behavioral, and biomedical sciences. *Behavior Research Methods*, *39*(2), 175–191. https://doi.org/10.3758/BF03193146

Gratton, G., Coles, M. G. H., & Donchin, E. (1983). A new method for off-line removal of ocular artifact. *Electroencephalography and Clinical Neurophysiology*, *55*(4), 468–484. https://doi.org/https://doi.org/10.1016/0013-4694(83)90135-9

H. N. Alexander Logemann, Koen B. E. Böcker, Peter K. H. Deschamps, C. K. and J. L. K. (2014). *The effect of attenuating noradrenergic neurotransmission by clonidine on brain activity measures of visuospatial attention*.

Harmon-Jones, E., Gable, P. A., & Peterson, C. K. (2010). The role of asymmetric frontal cortical

activity in emotion-related phenomena: A review and update. *Biological Psychology*, *84*(3), 451–462. https://doi.org/10.1016/j.biopsycho.2009.08.010

Heatherton, T. F., & Wagner, D. D. (2011). Cognitive neuroscience of self-regulation failure. *Trends in Cognitive Sciences*, *15*(3), 132–139. https://doi.org/10.1016/j.tics.2010.12.005

Houben, K., Nederkoorn, C., & Jansen, A. (2014). Eating on impulse: The relation between overweight and food-specific inhibitory control. *Obesity*, *22*(5), 2013–2015. https://doi.org/10.1002/oby.20670

IBM Corporation. (n.d.). *IBM SPSS Statistics for Windows* (No. 26). https://www.ibm.com/products/spss-statistics

Iyer, M. B., Mattu, U., Grafman, J., Lomarev, M., Sato, S., & Wassermann, E. M. (2005). Safety and cognitive effect of frontal DC brain polarization in healthy individuals. *Neurology*, *64*(5), 872 LP – 875. https://doi.org/10.1212/01.WNL.0000152986.07469.E9

Jasinska, A. J., Yasuda, M., Burant, C. F., Gregor, N., Khatri, S., Sweet, M., & Falk, E. B. (2012). Impulsivity and inhibitory control deficits are associated with unhealthy eating in young adults. *Appetite*, *59*(3), 738–747. https://doi.org/https://doi.org/10.1016/j.appet.2012.08.001

Johnstone, T., Van Reekum, C., Urry, H., Kalin, N., & Davidson, R. (2007). Johnstone T, van Reekum CM, Urry HL, Kalin NH, Davidson RJ. Failure to regulate: counterproductive recruitment of top-down prefrontal-subcortical circuitry in major depression. *Journal of Neuroscience,* 27: 8877-8884.https://doi.org/10.1523/JNEUROSCI.2063-07.2007

Kappenman, E., & Luck, S. (2012). *The Oxford Handbook of Event-Related Potential Components*. https://doi.org/10.1093/oxfordhb/9780195374148.001.0001

Kekic, M., McClelland, J., Bartholdy, S., Boysen, E., Musiat, P., Dalton, B., Tiza, M., David, A. S., Campbell, I. C., & Schmidt, U. (2017). Single-Session Transcranial Direct Current Stimulation Temporarily Improves Symptoms, Mood, and Self-Regulatory Control in Bulimia Nervosa: A Randomised Controlled Trial. *PLOS ONE*, *12*(1), e0167606. https://doi.org/10.1371/journal.pone.0167606

Kelley, N. J., Hortensius, R., Schutter, D. J. L. G., & Harmon-Jones, E. (2017). The relationship of approach/avoidance motivation and asymmetric frontal cortical activity: A review of studies manipulating frontal asymmetry. *International Journal of Psychophysiology*, *119*, 19–30. https://doi.org/10.1016/j.ijpsycho.2017.03.001

Laakso, I., Tanaka, S., Koyama, S., De Santis, V., & Hirata, A. (2015). Inter-subject Variability in Electric Fields of Motor Cortical tDCS. *Brain Stimulation*, *8*(5), 906–913. https://doi.org/https://doi.org/10.1016/j.brs.2015.05.002

Laakso, I., Tanaka, S., Mikkonen, M., Koyama, S., Sadato, N., & Hirata, A. (2016). Electric fields of motor and frontal tDCS in a standard brain space: A computer simulation study. *NeuroImage*, *137*. https://doi.org/10.1016/j.neuroimage.2016.05.032

Lansbergen, M., Böcker, K., Bekker, E., & Kenemans, J. (2007). Neural correlates of stopping and self-reported impulsivity. *Clinical Neurophysiology: Official Journal of the International Federation of Clinical Neurophysiology*, *118*, 2089–2103. https://doi.org/10.1016/j.clinph.2007.06.011

Logan, G. D., Cowan, W. B., & Davis, K. A. (1984). On the ability to inhibit simple and choice reaction time responses: A model and a method. *Journal of Experimental Psychology: Human Perception and Performance*, *10*(2), 276–291. https://doi.org/10.1037/0096-1523.10.2.276

Logemann, H.N.Alexander, Böcker, K., Deschamps, P., Kemner, C., & Kenemans, J. (2013). The effect of noradrenergic attenuation by clonidine on inhibition in the stop signal task. *Pharmacology, Biochemistry, and Behavior*, *110*.

https://doi.org/10.1016/j.pbb.2013.06.007

Logemann, H N A, Böcker, K. B. E., Deschamps, P. K. H., Harten, P. N. van, Koning, J., & Kemner, C. (2017). Haloperidol 2 mg impairs inhibition but not visuospatial attention. *Psychopharmacology*, *234*(2), 235–244.

Logemann, H N Alexander, Böcker, K. B. E., Deschamps, P. K. H., Kemner, C., & Kenemans, J. L. (2014). The effect of attenuating noradrenergic neurotransmission by clonidine on brain activity measures of visuospatial attention. *Human Psychopharmacology: Clinical and Experimental*, *29*(1), 46–54. https://doi.org/https://doi.org/10.1002/hup.2367

Luijten, M., Littel, M., & Franken, I. H. A. (2011). Deficits in Inhibitory Control in Smokers During a Go/NoGo Task: An Investigation Using Event-Related Brain Potentials. *PLOS ONE*, *6*(4), e18898. https://doi.org/10.1371/journal.pone.0018898

M.J.F. Robinson, A.M. Fischer, A. Ahuja, E. N. L. H. M. (2016). Roles of“Wanting”and“Liking”in Motivating Behavior: Gambling, Food,and Drug Addictions. *Current Topics in Behavioral Neurosciences*, *27*, 105–136. https://doi.org/10.1007/7854

Mangun, G., & Hillyard, S. (1991). Modulations of Sensory-Evoked Brain Potentials Indicate Changes in Perceptual Processing During Visual-Spatial Priming. *Journal of Experimental Psychology. Human Perception and Performance*, *17*, 1057–1074. https://doi.org/10.1037//0096-1523.17.4.1057

Mathôt, S., Schreij, D., & Theeuwes, J. (2012). OpenSesame: An open-source, graphical experiment builder for the social sciences. *Behavior Research Methods*, *44*(2), 314–324. https://doi.org/10.3758/s13428-011-0168-7

Meinke, A., Thiel, C., & Fink, G. R. (2006). Effects of nicotine on visuo-spatial selective attention as indexed by event-related potentials. *Neuroscience*, *141*, 201–212. https://doi.org/10.1016/j.neuroscience.2006.03.072

Monai, H., & Hirase, H. (2016). Astrocytic calcium activation in a mouse model of tDCS—Extended discussion. *Neurogenesis*, *3*(1), e1240055. https://doi.org/10.1080/23262133.2016.1240055

Monai, H., & Hirase, H. (2017). Astrocytes as a target of transcranial direct current stimulation (tDCS) to treat depression. *Neuroscience Research*, *126*. https://doi.org/10.1016/j.neures.2017.08.012

Monai, H., Ohkura, M., Tanaka, M., Oe, Y., Konno, A., Hirai, H., Mikoshiba, K., Itohara, S., Nakai, J., Iwai, Y., & Hirase, H. (2016). Calcium imaging reveals glial involvement in transcranial direct current stimulation-induced plasticity in mouse brain. *Nature Communications*, *7*(1), 11100. https://doi.org/10.1038/ncomms11100

Nexus-32. (n.d.). Mind Media. www.mindmedia.com

Opitz, A., Paulus, W., Will, S., Antunes, A., & Thielscher, A. (2015). Determinants of the electric field during transcranial direct current stimulation. *NeuroImage*, *109*. https://doi.org/10.1016/j.neuroimage.2015.01.033

Posner, M. I., Snyder, C. R., & Davidson, B. J. (1980). Attention and the detection of signals. *Journal of Experimental Psychology: General*, *109*(2), 160–174. https://doi.org/10.1037/0096-3445.109.2.160

R software: a tool analysing experimental data. (2016).

Saturnino, G., Antunes, A., & Thielscher, A. (2015). On the importance of electrode parameters for shaping electric field patterns generated by tDCS. *NeuroImage*, *120*. https://doi.org/10.1016/j.neuroimage.2015.06.067

Schestatsky, P., Morales-Quezada, L., & Fregni, F. (2013). Simultaneous EEG monitoring during transcranial direct current stimulation. *Journal of Visualized Experiments: JoVE*, *76*, 1–11. https://doi.org/10.3791/50426

Smith, E. E., Reznik, S. J., Stewart, J. L., & Allen, J. J. B. (2017). Assessing and conceptualizing frontal EEG asymmetry: An updated primer on recording, processing, analyzing, and interpreting frontal alpha asymmetry. *International Journal of Psychophysiology: Official Journal of the International Organization of Psychophysiology*, *111*, 98–114. https://doi.org/10.1016/j.ijpsycho.2016.11.005

Stoet, G. (2010). PsyToolkit: A software package for programming psychological experiments using Linux. *Behavior Research Methods*, *42*(4), 1096–1104. https://doi.org/10.3758/BRM.42.4.1096

Stoet, G. (2017). PsyToolkit: A Novel Web-Based Method for Running Online Questionnaires and Reaction-Time Experiments. *Teaching of Psychology*, *44*(1), 24–31. https://doi.org/10.1177/0098628316677643

Thiel, C., & Fink, G. (2008). Effects of the cholinergic agonist nicotine on reorienting of visual spatial attention and top-down attentional control. *Neuroscience*, *152*, 381–390. https://doi.org/10.1016/j.neuroscience.2007.10.061

Tremblay, S., Lepage, J., Latulipe-Loiselle, A., Fregni, F., Pascual-Leone, A., & Théoret, H. (2014). The Uncertain Outcome of Prefrontal tDCS. *Brain Stimulation*, *7*. https://doi.org/10.1016/j.brs.2014.10.003

Truong, D., Magerowski, G., Blackburn, G., Bikson, M., & Alonso-Alonso, M. (2013). Computational modeling of transcranial direct current stimulation (tDCS) in obesity: Impact of head fat and dose guidelines. *NeuroImage: Clinical*, *2*, 759–766. https://doi.org/10.1016/j.nicl.2013.05.011

Tsegaye, A., Guo, C., Stoet, G., Cserjési, R., Kökönyei, G., & Logemann, H. N. A. (2022). The relationship between reward context and inhibitory control, does it depend on BMI, maladaptive eating, and negative affect? *BMC Psychology*, *10*(1), 4. https://doi.org/10.1186/s40359-021-00712-5

Van Der Lubbe, R. H. J., Neggers, S. F. W., Verleger, R., & Kenemans, J. L. (2006). Spatiotemporal overlap between brain activation related to saccade preparation and attentional orienting. *Brain Research*, *1072*(1), 133–152. https://doi.org/10.1016/j.brainres.2005.11.087

Volkow, N. D., Wise, R. A., & Baler, R. (2017). The dopamine motive system: Implications for drug and food addiction. *Nature Reviews Neuroscience*, *18*(12), 741–752. https://doi.org/10.1038/nrn.2017.130