Light-driven synchronization of optogenetic clocks

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Abstract

Synthetic genetic oscillators can serve as internal clocks within engineered cells to program periodic expression. However, cell-to-cell variability introduces a dispersion in the characteristics of these clocks that drives the population to complete desynchronization. Here we introduce the optorepressilator, an optically controllable genetic clock that combines the repressilator, a three-node synthetic network in *E. coli*, with an optogenetic module enabling to reset, delay, or advance its phase using optical inputs. We demonstrate that a population of optorepressilators can be synchronized by transient green light exposure or entrained to oscillate indefinitely by a train of short pulses, through a mechanism reminiscent of natural circadian clocks. Furthermore, we investigate the system's response to detuned external stimuli observing multiple regimes of global synchronization. Integrating experiments and mathematical modeling, we show that the entrainment mechanism is robust and can be understood quantitatively from single cell to population level.

Introduction

Genetic clocks keep time within living organisms in order to program periodic behaviors like circadian rhythms. An intensive genetic analysis of the complex landscape of these biological oscillations has revealed that, from bacteria and fungi to plants and animals, these clocks share similar motifs in the underlying gene regulatory networks [1, 2]. From a reverse perspective, synthetic biologists have tackled the problem of designing from scratch minimal gene networks that can produce periodic patterns of gene expression [3–6]. Very early numerical simulations had shown that networks with an odd number of cyclically connected genes exhibit robust oscillations [7]. The repressilator was the first experimental realization of a synthetic genetic clock based on this principle [3]. As shown schematically in Fig. 1, the repressilator is a minimal network consisting of three transcription factors mutually repressing on a loop. The original design, using the repressors LacI, TetR and cI in *E. coli*, displayed marked oscillations in single cells, although with large fluctuations in both amplitude and period. This noise has been recently significantly reduced by genetic optimization, resulting in much more robust albeit slower oscillations [8]. This refactored repressilator is usually referred to as repressilator 2.0 [9]. In this system, the decrease in protein concentration is driven only by growth-related dilution, not by active protein degradation. As discussed in [3], a symmetric, protein only model already predicts limit cycle oscillations provided repression is steep enough:

$$\dot{x} = \frac{\beta}{1 + z^n} - \alpha x \qquad \dot{y} = \frac{\beta}{1 + x^n} - \alpha y \qquad \dot{z} = \frac{\beta}{1 + y^n} - \alpha z \qquad (1)$$

where x, y, z are the three repressors concentrations in units of the dissociation constant K, the concentration of proteins required to repress a promoter to half maximum, α is a common decay rate set by dilution and β is the normalized maximum production rate. In the digital approximation ($n \to \infty$), when $\beta/\alpha \gg 1$ the resulting dynamics look like relaxation oscillations with amplitude β/α and a full cycle period given by $T_0 = 3 \log(\beta/\alpha)/\alpha$ (see Fig. 1a and Supplementary Materials Section 1). As a result, although individual cells oscillate indefinitely, the natural dispersion of growth rates α results in a dispersion of periods leading to progressive dephasing of individual oscillators as shown by the simulations in Fig. 1b. In the same figure we report an experimental observation of this damping that we obtained using *E. coli* bacteria carrying the repressilator 2.0 [8]. This system contains three fluorescent reporters whose expression is regulated by the same three transcription factors of the repressilator, so that the reporters' concentration follows that of the repressor transcribed by the same promoter (see Fig. 1a). The cultures were initially synchronized chemically with IPTG, which deactivates the LacI repressor eliminating the edge between x and y from the network in Fig. 1a. This new topology admits a stable fixed point where the concentrations of x and y are maximal while z goes to zero. Next, the cultures were maintained in exponential growth phase by periodic dilutions in a multiwell plate while the population-averaged fluorescence signal was monitored using a plate reader (see Materials and Methods). For clarity reasons, we will often report

Fig. 1 Dephasing in a population of repressilators. a (left) Schematic representation of the repressilator 2.0 plasmid. (right) Simulated time evolution of the three repressors concentrations in the limit cycle of the protein-only model in Eq. 1. The reported expressions for amplitude and period are derived in the limits $n \to \infty$ and $\beta/\alpha \gg 1$ (see Supplementary Materials Section 1). **b** Concentration of the reporter CFP (TetR) as a function of time for an initially synchronized population of oscillators growing in a multi-well plate. Blue circles represent average over two technical replicates, corresponding errorbars are comparable to symbol size. The shadowed gray curves show simulations of independent oscillators (see Methods and Materials) and standard deviation $0.034 \, \text{h}^{-1}$. Dephasing due to the variability of oscillators periods causes a damping in the mean population signal reported as a blue line. Snapshots of the population ensemble in the 3D concentration space x-y-z are reported for three instants of time during the simulation, clearly showing progressive dephasing of individual oscillators over the limit cycle trajectory.

only the fluorescence signal from the CFP reporter that indirectly quantifies the concentration of the TetR repressor or y in our simple model. Fig. 1b shows that when starting from the synchronized state, the population signal from the CFP reporter displays high contrast oscillations with a period of 16 hours and an amplitude that is reduced to a half after about 2.5 periods. Phase drifts are very common in natural biological oscillators. Small couplings within a population of oscillators can give rise to a globally synchronized state [10], as in the case of cardiac pacemaker cells [11] or

quorum sensing coupled genetic oscillators [12, 13]. Other genetic oscillators, like circadian clocks, rely instead on a periodic external cue, known as zeitgeber (time-giver), to constantly adjust their phase to that of a common environmental cycle. Sunlight is the predominant zeitgeber of natural circadian clocks [14]. In the context of synthetic biology, light is a particularly versatile input for controlling the state of genetic circuits and programming gene expression in space and time with much greater precision than chemical signals [15–18]. Optical signals can also be multiplexed through spectral [19, 20] or amplitude modulation [21]. A growing number of optogenetics tools have been recently applied in prokaryotes to control different aspects of bacterial physiology [22], such as growth [23–25], antibiotic resistance [26], motility [27, 28] and adhesion [29]. A widely used optogenetic system is the light-switchable two-component system, CcaS-CcaR from *Synechocystis* PCC 6803 [30]. CcaS senses green light and phosphorilates the response regulator CcaR. Phosphorylated CcaR binds to the promoter $P_{cpcG2-172}$, activating gene expression. Red light reverts CcaS to the inactive state and shuts down transcription from $P_{cpcG2-172}$. This system was optimized for controllable gene expression with a high dynamic range in *E. coli* [31, 32].

Here we show that integrating an optogenetic module in the repressilator circuit enables the use of light to synchronize, entrain, and detune oscillations in gene expression within single cells or entire populations. We employ the CcaS-CcaR light-inducible system to express one of the repressilator proteins, resulting in a novel 4-node optogenetic network named the 'optorepressilator'. With this modification, light induces precise phase adjustments among synthetic genetic clocks within individual cells, leading to persistent population-wide oscillations. These oscillations mantain a constant phase relation to the external light cue that can act as a zeitgeber.

We show that a population of these synthetic oscillators can be synchronized through transient green light exposure or be entrained via a sequence of short pulses, sustaining indefinite oscillations. Additionally, we explore the system's response to detuned external stimuli, revealing multiple synchronization regimes.

Results

Optorepressilator: a light-controllable repressilator. In the optorepressilator (Fig. 2a), LacI proteins are produced by two genes. We indicate with x the normalized concentration of the repressilator's LacI, transcribed via the λ promoter and repressed by z (cI), and with x' the concentration of LacI proteins transcribed via the light-inducible promoter $P_{cpcG2-172}$ [31] (Fig. 2b). x and x' add up to repress protein y, while a light-dependent production rate drives x' dynamics:

$$\dot{x} = \frac{\beta}{1+z^n} - \alpha x, \;\; \dot{y} = \frac{\beta}{1+(x+x')^n} - \alpha y, \;\; \dot{z} = \frac{\beta}{1+y^n} - \alpha z, \;\; \dot{x}' = \beta' - \alpha x' \quad (2)$$

where β' is a light dependent production rate. It is important to note that the dynamics of x' is decoupled from all other repressors and only determined by light. In particular, under steady illumination conditions $x' = \beta'/\alpha$. If the expression of the light-inducible LacI is adjusted to have a dynamic range containing the dissociation

Fig. 2 The optorepressilator: a light-controllable genetic oscillator a Schematic illustration of the optorepressilator circuit. Green and red light respectively promote and repress the production of one of the three transcription factors in the repressilator (LacI). **b** Working mechanism of the optogenetic module. A light-driven two-component system controls the production of an additional copy of *lacI*. The optogenetic system consists of the membrane-associated histidine kinase CcaS and its response regulator CcaR. Absorption of green light increases the rate of CcaS autophosphorylation and phosphate transfer to the transcription factor CcaR. Phosphorylated CcaR promotes transcription of an additional copy of the LacI gene from the promoter $P_{cpcG2-172}$. Red light reverts CcaS to the inactive state and shuts down transcription from $P_{cpcG2-172}$. **c** Ideal optorepressilator's dynamics according to Eq. 2. The system oscillates unperturbed under red light, but collapses to a fixed point under green light when the extra x' represses y.

constant K, then we might be able to optically switch the system from limit cycle oscillations under red light to a fixed point under green light (Fig. 2**c**). In the digital approximation, the limit cycle is broken when $\beta'/\alpha > 1$ and the system collapses to a fixed point with coordinates $x_0 = 0, y_0 = 0, z_0 = \beta/\alpha$.

Fine-tuning optogenetic expression. Estimates for the LacI dissociation constant K vary between $0.01 - 0.1$ nM [33]. Even taking into account the fact that the repressor plasmid is present in more than one copy (~ 5 copies), this suggests that a small number of LacI proteins may already disrupt the limit cycle. Therefore, controlling the leakage of the promoter under the red light is crucial. The optogenetic module consists of two components, named as sensor and actuator in Fig. 3c. In order to fine-tune the expression of LacI, we created four different ranges of gene expression in which both transcription and translation were modulated on two levels. Translation was controlled by substituting the ribosome binding site (RBS) (BBa_B0034) in the original plasmid with a weaker RBS (BBa_B0033) from the same IGEM Community collection. Transcription was modulated through gene copy number by moving the light-driven gene expression cassettes from the plasmids to the genome. Combined with the sensor and actuator plasmids, these constructs resulted in four versions of the optogenetic

Fig. 3 Fine-tuning gene expression in the optorepressilator circuit. a To tune expression from the optogenetic module we varied the strength of RBSs and gene copy number by placing the output gene (sfGFP) either on a plasmid or in the chromosome. **b** Light-controlled expression levels of the sfGFP reporter from the four constructs in **a** and a negative control consisting of DHL708 with plasmids pNO286-3 and pSR58-0 (optogenetic plasmids without sfGFP cassette). For each curve, the samples were exposed to a fixed level of red light (intensity 0.74 W/m^2) while increasing green light intensity, as indicated by the dots' colors (color reference on the right). The main error bars represent the dynamic range of each sample. The smaller error bars represent the standard deviation of individual light conditions between replicates made in three separate days. The gray shaded area represents the autofluorescence background. Light intensities and raw fluorescence data are in Supplementary Figure 6. **c** Scheme of the final optorepressilator circuit (see Methods and Materials for details). **d** Time evolution of TetR reporter (CFP) concentration in a population of IPTG synchronized cells growing under red light. Black points from the original repressilator 2.0 display marked oscillations. Colored lines correspond to the four constructs in **a** with sfGFP replaced by LacI and the addition of the sponge promoters as in pSpongeROG. Circles represent data, where each dot is the average of two replicates with error bars comparable to marker size, while lines are spline interpolations. Only the purple line, corresponding to the system in **c**, shows oscillations comparable to those of the original repressilator. The difference in period can be explained by the difference in growth rate of the two strains, as shown in Supplementary Figure 4.

module (Fig. 3a) with different expression ranges. We characterized these expression ranges as a function of incident light (Fig. 3b) using sfGFP as fluorescent reporter and a custom-made light-addressable multiwell plate (see Supplementary Figure 3). By comparing expression at maximum green level, we can estimate that RBS substitution leads to a 27-fold decrease in reporter production (Fig. 3b), while relocation of the light-driven cassette to the genome reduces expression by 57-fold. The combination of weak RBS and genome insertion results in a gene expression range below the

autofluorescence background (estimated combined fold reduction of 1500). We then replaced the sfGFP gene with LacI in all four versions of the optogenetic module and transformed the repressilator plasmid (pLPT234) in each of the four strains. As a first step, we verified that the oscillations of the limit cycle were preserved under red light. To this end, we first chemically synchronized the oscillations with IPTG and then monitored the concentration of TetR (y) reported by CFP. Cultures were maintained in exponential phase by periodic dilutions in multiwells under constant red light. We found that only the strain with the lowest expression level (represented in Fig. 3**c**) oscillates with the same amplitude as the control strain containing only the repressilator plasmids (Fig. 3d). The slight difference in period can be explained by the presence of additional plasmids in the optorepressilator strain, which results in a lower growth rate. As found in the digital approximation, the repressilator period is mainly controlled by the inverse growth rate (see Fig. 1a and Supplementary Figure 9) meaning a lower growth rate results in a longer oscillation period. When we normalize the time with the growth rate the two oscillations overlap nicely (Supplementary Figure 4). In contrast, no clear oscillations were observed in the other three strains, where LacI leaking from the red-repressed promoter destroys the limit cycle and collapses all cells in a fixed point where the repressilator protein cI is high and TetR is low (see Supplementary Materials Section 5).

Optogenetic synchronization. Having verified that the system oscillates under red light, we then checked whether green light can synchronize a population of optorepressilators. Fig. 4**a** shows the population signal of CFP fluorescence reporting the concentration of TetR (y) in multiwell cultures. The cultures were constantly kept under red light for the first 40 hours. Although individual cells oscillate, their phases are randomly distributed so that the average population signal is constant. At $t = 40$ h we switch from red to green for 12 hours, and CFP fluorescence decays to zero. This is expected when extra LacI is produced by the optogenetic module, repressing both TetR and CFP. When the population signal decays completely, all the cells are stuck in the same fixed point ($x_0 = 0, y_0 = 0, z_0 = \beta/\alpha$ in the model), so that when switching back to red, they start oscillating in synchrony. This was also confirmed by single-cell data from a mother-machine microfluidic chip (Fig. 4**b**). Under the same light protocol as in Fig. 4**a**, most of the channels blink in unison after exposure and removal of synchronizing green light (Supplementary Video 1).

Optogenetic entrainment. Both plate reader and mother-machine experiments showed that cells carrying the optorepressilator system could be synchronized by transient light exposure. However, oscillations in the population signal were progressively dampened again by the dispersion of growth rates and thus of individual clocks' periods. This was particularly evident in the mother-machine experiment, where the growth rate variability is larger. Natural genetic clocks are able to counteract period dispersion by exploiting an external periodic stimulus to advance or delay their phases. For example, it was shown that a one-hour exposure to light at bedtime can delay the human circadian rhythm by about two hours, while exposure to the same intensity of white light after waking up can advance our schedule by a little less than half an hour [34]. Interestingly, the optorepressilator model in equation (2), despite its simplicity, displays a very similar behavior. In Fig. 5a we report the phase shift $\Delta\phi$

Fig. 4 Optical synchronization. a Time evolution of mSCFP3(CFP), mVenus and mKate2 signals from a population of exponentially growing cells in multiwell plate. Red and green shaded areas represent the illumination protocol. Dots reports data for optorepressilator cells and clearly shows the appearance of synchronous oscillations after transient illumination with green light, each marker is the average of two replicates and the error bar is data range. **b** Single cell data from a mother machine experiment employing the same light protocol as in a. The gray curves represent the concentration of CFP for individual cells growing in different channels, while the blue curve is their average. Snapshots above the plot report fluorescence imaging of bacteria in the microfluidic chip, centered at the corresponding time point on the time axis below.

produced by a single pulse (with a duration of 2 h and intensity $\beta' = 80$ h^{-1} fixed for all the simulations) as a function of the pulse arrival phase ϕ. This type of curve is often referred to as a phase response curve (PRC) and is obtained here by numerical integration of (2) for a single optorepressilator. The first thing we notice is that positive pulse arrival phase $\phi > 0$ results in a negative phase shift $\Delta\phi < 0$ that delays subsequent oscillations, while a negative ϕ results in a phase advance ($\Delta\phi > 0$). This behavior can be understood at least qualitatively by simple considerations. When a pulse arrives before y reaches the maximum ($\phi < 0$), a burst of x' is produced (Fig. 5b) that may trigger an earlier decay of y if $\beta'/\alpha > 1$ and the pulse duration τ is long enough. This results in an advanced peak, or equivalently a positive phase shift, which is greater the earlier the light pulse arrives. Conversely, when the pulse arrives while y is decaying the x' burst will prolong the y decay until the moment when x' falls below

1. This results in a delayed peak, or a negative phase shift that increases in magnitude as ϕ increases (Fig. 5b). The exact shape of the PRC will depend on light intensity through β' and pulse duration τ as shown in Supplementary Figure 7.

The phase response curve turns out to be a very useful concept to predict the system's response to a periodic external input. For example, if the system is exposed to a periodic train of light pulses, the phase response curve can be used to predict the sequence of phases ϕ_n at which subsequent pulses will arrive [35].

$$\phi_{n+1} = \phi_n + \frac{T_L}{T_0} - 1 + \Delta\phi(\phi_n) \tag{3}$$

where phases go from 0 at the expression peak of the y protein, to 1 when a full cycle is completed at the next peak. The fixed points ϕ^* of this mapping are those for which $\phi_{n+1} = \phi_n$ and hence:

$$\Delta\phi(\phi^*) = 1 - \frac{T_L}{T_0} \tag{4}$$

The fixed points where the phase response curve has a negative slope satisfying the condition $-2 < d\Delta\phi/d\phi < 0$, represent stable entrained states [35] for which the system oscillates at the same frequency of the external light signal. So when the system is exposed to a train of external pulses of period T_L we should look for the phase ϕ^* for which Eq.4 is satisfied, and if the phase response curve has a negative slope larger than -2, we can predict that the system will be entrained with a stable phase difference ϕ^* between light pulses and the peaks of CFP (y) protein.

Let us now consider an ensemble of optorepressilators with distributed natural periods T_0 and subjected to a train of light pulses with period T_L. Based on the previous discussion, each optorepressilator will be entrained by the external periodic signal but with a specific phase difference satisfying Eq.4. The population signal will then show entrained oscillations representing the average over individual oscillators having the same period but maintaining different phase differences with the external signal.

From this simplified theoretical discussion, we deduce that if real optorepressilators had the predicted phase response curve, then it should be possible to use a train of light pulses as a zeitgeber capable of producing long-term oscillations in gene expression at the population level. We first demonstrate this by monitoring the population signal from CFP (reporting TetR or y in the model) in multiwell cultures under constant red illumination (6.82 W/m^2) interrupted by green light pulses (5.64 W/m^2) of duration 2 h with period $T = 18$ h. Fig. 5d shows high contrast and undamped oscillations to be contrasted to the damped ones in Fig. 1b and Fig. 4a. The bottom panel in Fig. 5d shows the result of a numerical simulation with the same parameters as in Fig. 1b and the addition of a periodic light stimulation, with period $T_L/T_0 = 1$. Simulation panel also displays in gray the signals from individual optorepressilators before performing the average (in blue). These results are also confirmed by mother machine observations reported in Fig. 5e (Supplementary Video 2). For the simulations in the lower panel of Fig. 5e, all parameters remained the same as in Fig. 5d with the exception of the period of the light pulses ($T_L/T_0 = 0.97$) and the standard deviation of the growth rate distribution, which was increased from 0.034 h^{-1} to 0.071 h^{-1} to better reproduce the experimental observations in the mother machine. A

Fig. 5 Optical entrainment. a Phase shift as a function of pulse arrival phase. **b** Numerical simulations of equation (2) illustrating the effect of pulse arrival phase on the phase of optorepressilator oscillations. **c** Graphical illustration of the parameters used to describe the phase shift. **d** (top) CFP signal from a population of cells growing exponentially in 96 well plates that are exposed to a train of periodic pulses of green light. The population signal displays undamped oscillations demonstrating optical entrainment. (bottom) Numerical simulation of an ensemble of optorepressilators evolving according to equation (2) and with distributed growth rates (same parameters as in Fig. 1b). Pulses have a duration of $\tau = 2$ h and a relative period of $T_L/T_0 = 1$. Gray lines are individual oscillators while blue is the population average. **e** (top) Gray lines are CFP signals from single cells growing in a mother machine under periodic pulsed illumination. The blue curve is the average. (bottom) Numerical simulation with the same parameters as in **d** but a larger dispersion of growth rates and a slightly shorter relative period $T_L/T_0 = 0.97$ was required to match experiments above. In both data and simulation the magenta dotted curve highlights a slow oscillator (low growth rate and larger amplitude) entrained with a phase such as to receive the light pulse on the rising edge to anticipate the next oscillation. Magenta dashed lines highlight faster oscillators whose phase is such to receive the pulse on the decaying edge to delay the following oscillation.

narrower distribution of growth rates in multiwell cultures could be due to the fact that faster-growing bacteria outperform slower-growing cells in a competing environment, unlike in the mother machine where there is no competition between cells in different channels. The theoretical discussion above predicts that the individual oscillators will each find their own stable phase with respect to external pulses. The slower ones will arrange themselves to receive the pulse on the rising edge of the peak to reduce their period, while the faster ones will have the pulse arriving after the peak to increase their period. We confirm this in both experiments and simulations in Fig. 5e, where the individual traces of a slow (higher amplitude) and a fast (lower amplitude) oscillator have been highlighted with dotted and dashed lines respectively.

Detuning. In an entrained population, most oscillators are detuned from their natural frequency to that of the external signal. In this section we will explore detuning by starting with numerical simulations of our simple model in Eq. 2 and then comparing them with long-term observations of detuned optorepressilators in a plate reader experiment. Fig. 6a shows a 3D surface representing the ratio of the actual optorepressilator frequency $\nu = 1/T_0$ over external frequency $f = 1/T_L$ as a function of frequency and amplitude of the external signal β'. The ν value is obtained as the frequency of the main peak in the power spectrum of the simulated data. The plateaus in this graph are related to the so-called Arnold's tongues [10], *i.e.* regions of synchronization in the frequency/amplitude plane. On the cyan plateau, the system oscillates with the same frequency as the external signal, while there are also higher-order plateaus with a fractional value of the ratio f/ν_0 (see Supplementary Figure 8). On the cyan tongue, when the system is detuned to higher frequencies, its phase will be such that it receives the light pulse on the rising edge of the y protein. When detuned to lower frequencies, however, it shifts to receive pulses on the falling edge of y. When detuning to lower frequencies, the system goes to an higher order synchronization tongue where it oscillates at twice the frequency of the external signal. Similarly, forcing to higher frequencies moves the system to fractional order tongues, such as the green plateau in the plot, in which the system oscillates at half the external frequency. All these regimes are found in experiments in which we maintain cultures of optorepressilators in exponential phase within multiwell plates that are independently addressed with light signals of different frequencies (Fig. 6b). It is also remarkable to observe how the relative phase between the system and the external signal evolves within the cyan tongue, as predicted by the model. More quantitatively, we have extracted the phase difference ϕ^* between light pulses and CFP oscillations from the data shown in the three central panels of Fig. 6b ($f = 0.8, 1, 1.2$). We found that, in accordance with the discussion in the previous section (Eq. 4), the red points with coordinates ($\phi^*, 1 - T_L/T_0$) fall on the theoretical phase response curve when we choose $\beta' = 80 \text{ h}^{-1}$ (Fig.5a).

A discrepancy is apparently found in the green tongue, where we experimentally observe oscillations at the same frequency as the external signal. This is not unexpected, however, when one realizes that although the individual optorepressilators may oscillate at half the external frequency f, they can peak at either the even or odd peaks of the external signal. When we average these alternating peaks over the population we get a small amplitude oscillation at the frequency of the external signal. This is also confirmed by a mother machine experiment where we tried to detune to

about twice the natural frequency and observed different channels oscillating at half the signal frequency and with alternating peaks (Fig. 6c).

Fig. 6 Detuning. a 3D surface representing the ratio between the actual frequency of a single forced optorepressilator and the frequency of the forcing signal, as a function of the forcing frequency and amplitude. The colors of the plateaus (Arnold's tongues) highlight different regions of global synchronization in the frequency/amplitude plane. **b** Time evolution of the average CFP concentration (blue curve) in a plate reader experiment, for different frequencies of green light pulses (green bars). The color bars at the right of the plot indicates the corresponding region on the surface in **a**. **c** Mother machine experiment revealing two distinct cells oscillating at half the signal frequency but peaking on alternate pulses of incoming light. This explains why for $f = 1.5$ and $f = 2$ in **b** we observe a population mean oscillating with the same frequency of the forcing instead of the $\nu/f = 0.5$ value predicted for the green tongue in **a**.

Discussion

Inspired by the light entrainment of natural circadian rhythms, we designed the optorepressilator, a four-node synthetic oscillatory network that can lock its phase to an external periodic light signal. By integrating an optogenetic module into a repressilator circuit, we demonstrate, theoretically and with experiments, that light can synchronize, entrain, and detune oscillations within single cells or an entire population. We find that this four-node network shows a phase-sensitive response to light pulses. Depending on the arrival time, a pulse can either delay or advance the clock as in many natural circadian clocks. As a result, our system can be entrained by periodic light pulses, even when the forcing period deviates from the natural frequency. Using a combination of

optogenetic experiments ranging from the macroscopic population scale to the microscopic scale of single cells, we show that the entrainment mechanism is robust and can be understood quantitatively by a simple protein-only model. The entrainment of biological clocks can provide new insights into oscillation mechanisms and, at the same time, practical means to control biological rhythms. Through periodic modulation of chemical signals within microfluidic environments, entrainment of natural biological clocks ranging from the embryonic segmentation clock [36] to the NF-kB system regulating immune response [37] has been previously achieved. However, the complexity of the underlying genetic networks often precludes a deeper mathematical understanding of the fundamental nature of the entrainment phenomenon. Synthetic oscillators provide an ideal platform for studying entrainment in engineered minimal systems where a close comparison with relatively simple models is possible [38]. Our minimal optorepressilator model can provide many theoretical predictions, often in analytical form within the digital approximation ($n \to \infty$). It explains correlations between amplitude and period of oscillations (Supplementary Figure 9), or how robust oscillations are against leakage (Supplementary Materials Section 5). Moreover an approximate form for the phase response curve is derived (Supplementary Materials Section 7), providing a quantitative physical insight into the mechanisms that produce delayed or advanced oscillations and on how pulse characteristics affect the system's response.

From a more applied perspective, the optorepressilator enriches the toolbox of genetic modules by adding a light-synchronizable clock that could be used to program precise oscillatory patterns of gene expression. When compared to chemical signaling, the use of light to control and coordinate the functioning of synthetic networks offers clear advantages in terms of spatial and temporal modulation. Light cues can be applied and removed on the spot, without waiting for media substitution [39]. In addition, using spatial light modulators it could be possible to address spatially separated subpopulations within a common environment to oscillate with distinct periods and phases. Optical synchronization of genetic oscillators can be easily implemented in a wide range of experimental settings like liquid cultures, agar plates or microfluidics. Light, for example, can penetrate bioreactors and orchestrate gene expression in a population of uncoupled oscillators. Moving to infrared inducible optogenetic systems [40], optical signals could also penetrate biological tissues for *in vivo* applications [9].

Materials and Methods

Strains and plasmids. A list of the strains and plasmids used is in Supplementary Table 1 and 2, along with plasmids maps and their description (Supplementary Figure 10 and 11). Genome insertion of light-driven cassettes was performed using lambda-red recombination [41] targeting the *attB* genome site. The starting strain was *E. coli* DHL708 (a gift from Johan Paulsson, Addgene plasmid # 98417) [8] for all insertions. All the recombination cassettes were amplified from modified versions of plasmid pKD46 [41] (Supplementary Table 2). In addition to kanamycin antibiotic resistance, the recombination cassettes contained the desired protein gene (LacI, sfGFP) controlled by the light-driven promoter $P_{cpcG2-172}$.

Plasmid cloning was performed using In-Fusion cloning (Takara Bio) for large rearrangements and Q5® Site-Directed Mutagenesis Kit (New England BioLabs) for small modifications *i. e.* RBS changes. The final optorepressilator system is composed of: the strain MCC0233 obtained inserting $P_{cpcG2-172}$ (the light-driven promoter), a weak RBS and LacI open reading frame in the genome of DHL708; pNO286-3 (a gift from Jeffrey Tabor, Addgene plasmid # 107746; http://n2t.net/addgene:107746; RRID:Addgene_107746) [32], plasmid with mini-CcaS light sensor and the enzymes for the phycocyanobilin chromophore; pLPT234 (a gift from Johan Paulsson, Addgene plasmid # 127855; http://n2t.net/addgene:127855; RRID:Addgene_127855) [9], plasmid with the core repressilator circuit and reporters; pSpongeROG, a modified version of plasmid pSR58.6 (a gift from Jeffrey Tabor, Addgene plasmid # 63176; http://n2t.net/addgene:63176; RRID:Addgene_63176) [19] added with the sponge from plasmid pLPT145 (a gift from Johan Paulsson, Addgene plasmid # 85527; http://n2t.net/addgene:85527; RRID:Addgene_85527) [8] and without the light-driven gene expression cassette (sfGFP).

Plate reader experiments to follow circuit oscillations. Bacterial strains were grown from glycerol stock for 16 hours in LB with appropriate antibiotics (see Supplementary Table 3 for antibiotic working concentration), in a falcon tube exposed to saturating 660 nm red light in a shaker incubator (200 rpm) at 37 °C. Cultures were diluted $1 : 10^6$ approximately 8 hours before the beginning of the experiment in imaging medium [8] with antibiotics under red light, and 1 mM IPTG was added in this interval if samples had to be chemically synchronized. Samples were transferred in duplicates to a 96-well plate (Greiner GR655096), and we measured OD600 and fluorescence for sCFP, mVenus and mKate2. When OD600 reached approximately 0.8 for the first time, the samples were diluted 1:4 in new wells with imaging medium plus antibiotics. Every two hours, we measured OD600 and fluorescence and diluted about 1:4 in fresh culture medium plus antibiotics to bring the cultures back to an OD of 0.2 and keep the bacteria under exponential growth conditions. OD600 and fluorescence were measured with a TECAN Infinite M Nano+ plate reader warmed to 37 °C. The parameters to detect fluorescence were: mSCFP3 excitation 433 ($\pm$9) nm emission 474 ($\pm$20) nm; mVenus excitation 500 ($\pm$9) nm emission 540 ($\pm$20) nm; mKate2 excitation 588 ($\pm$9) nm emission 633 ($\pm$20) nm. Between measurements, the well plate was kept in a shaking incubator (100 rpm) at 37 °C and individual wells were exposed to the appropriate light conditions through the custom-made light-addressable multiwell plate (Supplementary Figure 3). The red and green light intensities were respectively: 9.82 W/m^2, 5.64 W/m^2.

Data were analysed through custom python script. Blank absorbance of the medium was removed. Absorbance was then used to normalize fluorescence with respect to cell count.

Plate reader experiments to detect constructs expression range. Samples were grown from glycerol stocks overnight as in the previous protocol. Cells were refreshed in imaging medium plus antibiotics and OD600 was set to 0.002. Samples were transferred to a 96-well plate and placed in a shaking incubator at 37°C. There, individual wells were exposed to homogeneous levels of red light and a gradient of green light with the custom device in Supplementary Fig. 3. Absorbance and sfGFP

fluorescence were measured every hour by temporarily moving the plate from the incubator to the plate reader. Data were analysed through custom python script. Protein production rate was calculated as the time derivative of sfGFP concentration divided by OD600 in a selected OD600 interval of exponential growth.

Mother machine fabrication. Master molds with mother machine features were fabricated using a hybrid technique involving standard soft-lithography and two-photon polymerization [42]. Firstly, the feeding channel (50 μm-width, 15 μm-height) was fabricated using standard protocols of soft-lithography. Precisely, a SU-8 layer of 15 μm was fabricated by spinning SU-8 2015 onto a soda-lime coverglass (3000 rpm - 30 s, Laurell WS-650Mz-23NPPB). Strong adhesion of the SU8 to the carrier coverglass was ensured by three layers of OmniCoat adhesion promoter (MicroChem Corp). The coverglass was soft-baked, and a microfluidic mask with a pattern of 50 μm-wide channels was projected onto the photoresist (UV KUB 2, 400 mJ - 40 s at 25% of maximum power). The coverglass was soft-baked, post-baked, and developed according to the protocol provided by MicroChem Corp. In addition, the sample was hard-baked for 30 min at 170 ^{o}C. A second layer of 20 μm was fabricated on top of the feeding channel by spinning SU-8 2015 at 2000 rpm, followed by a soft-baking of 2 hours at 95 ^{o}C. Then, the microfabrication of the micron-size channels was carried out by a custom-built two-photon polymerization setup [43]. The refractive index contrast between cured and uncured SU-8 was used to identify the edge of the largest channel, where a comb of micrometer-sized channels was made by direct laser writing. The whole coverglass was again baked at 95 ^{o}C and rinsed with PGMEA and IPA. Finally, the master mold was silanized to prevent the PDMS from adhering to the master. PDMS was prepared from a Sylgard 184 Silicone Elastomer kit: polymer base and curing agent were mixed in a 10:1 ratio, and air bubbles were removed from the mixture by centrifugation. The degassed mixture was then poured over the master, and the devices were cured for about 1.5 hours at 90 ^{o}C. PDMS chips were peeled from the master mold and bonded to glass by oxygen plasma treatment (15 seconds at 100 watts) and then baked for 10 minutes at 120 ^{o}C.

Microscopy. Phase contrast and epi-fluorescence imaging were performed using a custom-built optical microscope equipped with a 100× magnification objective (Nikon MRH11902; NA=1.3) and a high-sensitivity CMOS camera (Hamamatsu Orca-Flash 4.0 V3) (see Supplementary Figure 12). For phase contrast imaging, a deep red LED (Thorlabs M730L4) with low inhibition of the optogenetic expression system was used. Light control was achieved by directing light through a 10:90 beam splitter (R:T, Thorlabs BSN10R) positioned under the objective. Green and red light stimuli were provided by two LEDs (Thorlabs M530L4, Thorlabs M660L4, respectively) coupled through a dichroic mirror (Thorlabs DMLP567R) and passing through a long-pass filter at 550 nm (Thorlabs FELH0550). Epi-fluorescence imaging was conducted using a blue LED (Thorlabs M455L4) and a filter set for the CFP (Chroma 49001-ET-ECFP). To enable imaging in both phase contrast and epi-fluorescence, a motorized filter wheel (Thorlabs FW102C) was used to switch between the fluorescence filter set and a long-pass filter at 700 nm (Thorlabs FWLH0700). To maintain sample focus throughout the entire acquisition process, a custom script was developed. This script scans the sample in height and finally moves to the z-plane where the image

of a specific fixed structure in the chip has maximum edge enhancement (calculated with the Sobel function). To avoid drift on the x-y plane, we correlate the acquired image of the fixed structure with one acquired at the beginning of the experiment and compute the shift on the x-y plane. The scanning process was performed using a motorized vertical lift stage (Zaber X-VSR-E) and a motorized microscope stage (Zaber X-ASR100B120B-SE03D12).

Mother machine experiments. Cells were grown from a glycerol stock for 16 hours in LB with appropriate antibiotics, in a 50 mL centrifuge tube exposed to saturating 660 nm red light. Bacteria were refreshed 1:100 in imaging medium under red light until they reached an OD of 0.1 (around 4 hours). 1 mL of culture was centrifuged in an Eppendorf miniSpin Plus centrifuge at 1000 rcf for 5 minutes and concentrated 50x. 20 μL of concentrated bacteria were loaded in the mothermachine's flow channel with a pipette. Bacteria were loaded in the growth channels, by centrifugation of the mothermachine chip for 7 minutes at 1300 rcf (with soft ramp acceleration) in an Eppendorf Centrifuge 5430R using the Combislide adapter. The flow channel of the mothermachine was then washed for approximately 5 minutes with LB with antibiotics and 0.1% BSA at a constant flow of 50 μL/min, to carry away excess bacteria. For the whole duration of the experiments, the mothermachine was perfused with LB with antibiotics and 0.1% BSA at a constant rate of 5.5 μL/min. Green and red light stimuli were provided by the two LEDs (Thorlabs M530L4, Thorlabs M660L4) with respective intensities 6 W/m^2 and 26 W/m^2 for the synchronization experiments, and 1.1 W/m^2 and 4.5 W/m^2 for the entrainment experiments.

Data analysis: segmentation in the mother machine. Phase contrast images were taken every 3 min and fluorescence images every 9 min. Phase contrast images were analyzed, to identify the single feeding channels of the microfluidic chip. Single cells were segmented using the pretrained neural network model Cellpose 2.0. We further trained the model with our own data to increase the accuracy of segmentation [44]. The masks obtained after segmentation were used to measure the total fluorescence of the mother cell in all feeding channels of the mother machine as a function of time.

Simulations. All simulations were performed by direct Euler integration of Eq. 2 using custom Python program. The selection of model parameters was motivated as follows: the mean value of the growth rate was directly estimated from experiments $\alpha = 0.75\text{h}^{-1}$ (Supplementary Figure 2); for all promoters we choose a cooperativity index $n = 3$ to both match experimental oscillation profiles and in agreement with [8]; for the production rates we chose the value $\beta = 300 \text{ h}^{-1}$ to match the experimental period $T_0 \simeq 17.5$ h; the maximum light induced production rate $\beta' = 80 \text{ h}^{-1}$ was estimated to maximize agreement with experimental data in Fig. 5a.

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Author contributions. R.D.L. conceived the project. M.C.C. designed and constructed all plasmids and strains, with G.F. and F.L. collaborating to plasmid design. N.P. developed mothermachine chips. G.F. and R.D.L. designed optics. M.C.C., G.F.,

and F.L. conducted experiments and analysed the data, with N.P. contributing specifically to the mothermachine's experiments and analysis. All the experiments have been performed under the supervision of G.F. and R.D.L. M.C.C., F.L., R.D.L. carried out simulations. All authors contributed to the writing of the manuscript.

Competing interests. The authors declare no competing interests.

References

[1] Young, M.W., Kay, S.A.: Time zones: A comparative genetics of circadian clocks. Nature Reviews Genetics **2**(9), 702–715 (2001) https://doi.org/10.1038/35088576

[2] Cookson, N.A., Tsimring, L.S., Hasty, J.: The pedestrian watchmaker: Genetic clocks from engineered oscillators. FEBS Letters **583**(24), 3931–3937 (2009) https://doi.org/10.1016/j.febslet.2009.10.089

[3] Elowitz, M.B., Leibler, S.: A synthetic oscillatory network of transcriptional regulators. Nature **403**(6767), 335–338 (2000) https://doi.org/10.1038/35002125

[4] Atkinson, M.R., Savageau, M.A., Myers, J.T., Ninfa, A.J.: Development of genetic circuitry exhibiting toggle switch or oscillatory behavior in escherichia coli. Cell **113**(5), 597–607 (2003)

[5] Stricker, J., Cookson, S., Bennett, M.R., Mather, W.H., Tsimring, L.S., Hasty, J.: A fast, robust and tunable synthetic gene oscillator. Nature **456**(7221), 516–519 (2008)

[6] Purcell, O., Savery, N.J., Grierson, C.S., Di Bernardo, M.: A comparative analysis of synthetic genetic oscillators. Journal of the Royal Society Interface **7**(52), 1503–1524 (2010) https://doi.org/10.1098/rsif.2010.0183

[7] Fraser, A., Tiwari, J.: Genetical feedback-repression. II. Cyclic genetic systems. Journal of Theoretical Biology **47**(2), 397–412 (1974) https://doi.org/10.1016/0022-5193(74)90206-9

[8] Potvin-Trottier, L., Lord, N.D., Vinnicombe, G., Paulsson, J.: Synchronous long-term oscillations in a synthetic gene circuit. Nature Letters **538**, 514–517 (2016)

[9] Riglar, D.T., Richmond, D.L., Potvin-Trottier, L., Verdegaal, A.A., Naydich, A.D., Bakshi, S., Leoncini, E., Lyon, L.G., Paulsson, J., Silver, P.A.: Bacterial variability in the mammalian gut captured by a single-cell synthetic oscillator. Nature Communications **10**(1), 1–12 (2019) https://doi.org/10.1038/s41467-019-12638-z

[10] Pikovsky, A., Rosenblum, M., Kurths, J.: Synchronization: a universal concept in nonlinear science. American Association of Physics Teachers (2002)

[11] Mirollo, R.E., Strogatz, S.H.: Synchronization of pulse-coupled biological oscillators. SIAM Journal on Applied Mathematics **50**(6), 1645–1662 (1990)

[12] Danino, T., Mondragón-Palomino, O., Tsimring, L., Hasty, J.: A synchronized quorum of genetic clocks. Nature **463**, 326–330 (2010)

[13] Prindle, A., Samayoa, P., Razinkov, I., Danino, T., Tsimring, L.S., Hasty, J.: A sensing array of radically coupled genetic 'biopixels'. Nature **481**(7379), 39–44 (2012)

[14] Golombek, D.A., Rosenstein, R.E.: Physiology of circadian entrainment (2010). https://doi.org/10.1152/physrev.00009.2009

[15] Levskaya, A., Chevalier, A.A., Tabor, J.J., Simpson, Z.B., Lavery, L.A., Levy, M., Davidson, E.A., Scouras, A., Ellington, A.D., Marcotte, E.M., *et al.*: Engineering escherichia coli to see light. Nature **438**(7067), 441–442 (2005)

[16] Tabor, J.J., Salis, H.M., Simpson, Z.B., Chevalier, A.A., Levskaya, A., Marcotte, E.M., Voigt, C.A., Ellington, A.D.: A synthetic genetic edge detection program. Cell **137**(7), 1272–1281 (2009)

[17] Olson, E.J., Hartsough, L.A., Landry, B.P., Shroff, R., Tabor, J.J.: Characterizing bacterial gene circuit dynamics with optically programmed gene expression signals. Nature methods **11**(4), 449–455 (2014)

[18] Baumschlager, A., Khammash, M.: Synthetic biological approaches for optogenetics and tools for transcriptional light-control in bacteria. Advanced Biology **5**(5), 2000256 (2021)

[19] Schmidl, S.R., Sheth, R.U., Wu, A., Tabor, J.J.: Refactoring and optimization of light-switchable escherichia coli two-component systems. ACS Synthetic Biology (2014)

[20] Fernandez-Rodriguez, J., Moser, F., Song, M., Voigt, C.A.: Engineering rgb color vision into escherichia coli. Nature chemical biology **13**(7), 706–708 (2017)

[21] Benzinger, D., Ovinnikov, S., Khammash, M.: Synthetic gene networks recapitulate dynamic signal decoding and differential gene expression. Cell Systems **13**(5), 353–364 (2022)

[22] Liu, Z., Zhang, J., Jin, J., Geng, Z., Qi, Q., Liang, Q.: Programming bacteria with light—sensors and applications in synthetic biology. Frontiers in microbiology **9**, 2692 (2018)

[23] Davidson, E.A., Basu, A.S., Bayer, T.S.: Programming microbes using pulse width modulation of optical signals. Journal of molecular biology **425**(22), 4161–4166 (2013)

[24] Milias-Argeitis, A., Rullan, M., Aoki, S.K., Buchmann, P., Khammash, M.: Automated optogenetic feedback control for precise and robust regulation of gene expression and cell growth. Nature communications **7**(1), 12546 (2016)

[25] Gutiérrez Mena, J., Kumar, S., Khammash, M.: Dynamic cybergenetic control of bacterial co-culture composition via optogenetic feedback. Nature Communications **13**(1), 4808 (2022)

[26] Sheets, M.B., Tague, N., Dunlop, M.J.: An optogenetic toolkit for light-inducible antibiotic resistance. Nature Communications **14**(1), 1034 (2023)

[27] Frangipane, G., Dell'Arciprete, D., Petracchini, S., Maggi, C., Saglimbeni, F., Bianchi, S., Vizsnyiczai, G., Bernardini, M.L., Di Leonardo, R.: Dynamic density shaping of photokinetic e. coli. Elife **7**, 36608 (2018)

[28] Zhang, J., Luo, Y., Poh, C.L.: Blue light-directed cell migration, aggregation, and patterning. Journal of molecular biology **432**(10), 3137–3148 (2020)

[29] Jin, X., Riedel-Kruse, I.H.: Biofilm lithography enables high-resolution cell patterning via optogenetic adhesin expression. Proceedings of the National Academy of Sciences **115**(14), 3698–3703 (2018)

[30] Tabor, J.J., Levskaya, A., Voigt, C.A.: Multichromatic control of gene expression in escherichia coli. Journal of Molecular Biology **405**, 315–324 (2011)

[31] Schmidl, S.R., Sheth, R.U., Wu, A., Tabor, J.J.: Refactoring and optimization of light-switchable escherichia coli two-component systems. ACS Synthetic Biology **3**(11), 820–831 (2014)

[32] Ong, N.T., Tabor, J.J.: A miniaturized escherichia coli green light sensor with high dynamic range. ChemBioChem **19**(12), 1255–1258 (2018)

[33] Ozbudak, E.M., Thattai, M., Lim, H.N., Shraiman, B.I., Van Oudenaarden, A.: Multistability in the lactose utilization network of escherichia coli. Nature **427**(6976), 737–740 (2004)

[34] St Hilaire, M.A., Gooley, J.J., Khalsa, S.B.S., Kronauer, R.E., Czeisler, C.A., Lockley, S.W.: Human phase response curve to a 1 h pulse of bright white light. The Journal of physiology **590**(13), 3035–3045 (2012)

[35] Granada, A., Hennig, R.M., Ronacher, B., Kramer, A., Herzel, H.: Chapter 1 Phase Response Curves, vol. 454, pp. 1–27. Elsevier, ??? (2009). https://doi.org/10.1016/S0076-6879(08)03801-9 . https://linkinghub.elsevier.com/retrieve/pii/S0076687908038019

[36] Sanchez, P.G.L., Mochulska, V., Mauffette Denis, C., Mönke, G., Tomita, T., Tsuchida-Straeten, N., Petersen, Y., Sonnen, K., François, P., Aulehla, A.: Arnold

tongue entrainment reveals dynamical principles of the embryonic segmentation clock. eLife **11**, 79575 (2022) https://doi.org/10.7554/eLife.79575

[37] Heltberg, M., Kellogg, R.A., Krishna, S., Tay, S., Jensen, M.H.: Noise induces hopping between nf-b entrainment modes. Cell Systems **3**(6), 532–5393 (2016) https://doi.org/10.1016/j.cels.2016.11.014

[38] Mondragón-Palomino, O., Danino, T., Selimkhanov, J., Tsimring, L., Hasty, J.: Entrainment of a population of synthetic genetic oscillators. Science **333**(6047), 1315–1319 (2011)

[39] Zhao, E.M., Yanfei Zhang, Y., Mehl, J., Park, H., Lalwani, M.A., Toettcher, J.E., Avalos, J.L.: Optogenetic regulation of engineered cellular metabolism for microbial chemical production. Nature (2018)

[40] Chernov, K.G., Redchuk, T.A., Omelina, E.S., Verkhusha, V.V.: Near-infrared fluorescent proteins, biosensors, and optogenetic tools engineered from phytochromes. Chemical Reviews **117**(9), 6423–6446 (2017) https://doi.org/10.1021/acs.chemrev.6b00700

[41] Datsenko, K.A., Wanner, B.L.: One-step inactivation of chromosomal genes in escherichia coli k-12 using pcr products. Proceedings of the National Academy of Sciences of the United States of America **97**(12), 6640–6645 (2000)

[42] Vanderpoorten, O., Peter, Q., Challa, P.K., Keyser, U.F., Baumberg, J., Kaminski, C.F., Knowles, T.P.: Scalable integration of nano-, and microfluidics with hybrid two-photon lithography. Microsystems & nanoengineering **5**(1), 1–9 (2019)

[43] Vizsnyiczai, G., Frangipane, G., Maggi, C., Saglimbeni, F., Bianchi, S., Di Leonardo, R.: Light controlled 3d micromotors powered by bacteria. Nature communications **8**(1), 1–7 (2017)

[44] Pachitariu, M., Stringer, C.: Cellpose 2.0: how to train your own model. Nature Methods **19**, 1634–1641 (2022)

Supplementary Materials for
Light-driven synchronization of optogenetic clocks

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Contents

1 Analytical solution of repressilator dynamics in the digital approximation

In the digital approximation, Hill functions in Eq. 1 in the main text are replaced by Θ functions and equations become piecewise linear first order. Oscillations are therefore built by joining together rising (to steady value β/α) or decaying (to 0) exponentials with rate α, calling with M and m respectively the maximum and minimum values in the oscillations. t is the interval between two maxima of two different proteins and δ is the time interval to rise from the minimum m to 1 (Fig. 1). All concentrations are measured in units of K so 1 represents the activation threshold. We can write the following four equations in the unknowns m, M, t, δ:

Fig. 1 Simulations of the digital model. M and m, respectively, are the maximum and minimum values in the oscillations and δ is the time interval to rise from the minimum m to 1 (threshold value in K units).

$$Me^{-(t-\delta)} = 1 \tag{1}$$

$$e^{-(t+\delta)} = m \tag{2}$$

$$\beta + (1-\beta)e^{-t} = M \tag{3}$$

$$\beta + (m-\beta)e^{-\delta} = M \tag{4}$$

Where, for simplicity of notation, we measure time in units of α^{-1}.
From Eq.(1) and (2) we find:

$$e^{-2t} = m/M \tag{5}$$

and

$$e^{-2\delta} = Mm \tag{6}$$

which substituted in (3) and (4) give:

$$\beta + (1 - \beta)\sqrt{m/M} = M \tag{7}$$

$$\beta + (m - \beta)\sqrt{Mm} = 1 \tag{8}$$

The two equations above can be solved numerically to get M and m once β is known. However if, as in our case, $\beta \gg 1$ we can find the approximate solutions:

$$M = \beta , \quad m = 1/\beta \tag{9}$$

Substituting back in (5) we get

$$t = \log \beta \tag{10}$$

and thus for the entire period

$$T = 3t = 3 \log \beta \tag{11}$$

Finally reintroducing the time scale α we can write for the period

$$T = \frac{3}{\alpha} \log \frac{\beta}{\alpha} \tag{12}$$

2 Growth rate estimate

Growth rate analysis of the optorepressilator data displayed in Figure 6b in the main text.

Fig. 2 **a** Raw absorbance data from one individual sample in the plate reader experiment. The initial gray area is removed from further analysis to ensure samples reached stable growth conditions. **b** Minimum and maximum OD600 points (respectively in yellow and red) in log scale are fitted with a line to extract the growth rate as its slope. **c** Distribution of the growth rates. Median and mean of the distribution are shown respectively in black and orange. Due to the non-symmetric distribution, we used the median to summarize the growth rate. **d** Box plots of the growth rates for each sample, all grown in parallel. The blue line inside the box plots is the median. The black line is the mean of all medians, our estimate growth rate $(0.75 \pm 0.01h^{-}1)$ for the optorepressilator in plate reader experiments. The gray area represents the mean growth rate $\pm$ the standard deviation.

3 Custom-made light-addressable multiwell plate

The custom-made light-addressable multiwell plate was made using an Adafruit NeoPixel NeoMatrix 8x8, a matrix of 64 RGB LEDs, attached to the bottom of a Greiner 96 well plate with black wells and removed bottoms (Supplementary Fig. 3a). The matrix was placed so that each LED was directly under an individual well. An opaque foam layer was cut in order to accommodate LEDs, adjusting the matrix to the plate and reducing well-to-well light contamination. An additional plate was fixed on top of this structure to decrease light intensity on samples by increasing the distance between LEDs and samples. Opaque foam layers were cut in correspondence with the wells and attached above and below this plate, again to avoid well-to-well light contamination. The construct was fixed to a shaking incubator (Supplementary Fig. 3b). A 96 well plate could be placed on top of it and removed for data acquisition. A darkened lid was placed on the samples' plate to block environment light.
The LEDs matrix was controlled with an Arduino microcontroller. To ensure correct timing of inputs, we employed an AZDelivery Real Time Clock module.
LEDs intensity on samples was measured with Thorlabs Standard Photodiode Power Sensor S121C.

Fig. 3 **a** Scheme of a longitudinal section of the device, with key components highlighted. **b** Frontal picture of the custom-made light-addressable multiwell plate placed in a shaking incubator. The sample plate and dark lid are partially lifted. **c** Top-down picture of the device. Dark lid and sample plate are removed and LEDs are on.

4 Period normalized by growth rate

Fig. 4 **a** Fluorescence intensities of the repressilator and optorepressilator, as shown in Figure 3d. **b** Time axis rescaled: time points of samples in **a** multiplied by their respective growth rates α (0.87 h^{-1}, 0.76 h^{-1}) and aligned to a common initial time. Post-rescaling, the oscillations of the repressilator and optorepressilator overlap nicely.

5 Effect of leakage on the period and stability of the oscillations

Leakage from the optogenetic x' promoter can destroy limit cycle oscillations and collapse the system into a stable fixed point. To study how leakage affects oscillations we employ linear stability analysis. In the absence of leakage ($\beta' = 0$), the system of equations is symmetric and the fixed point is (ξ_0, ξ_0, ξ_0), where ξ_0 satisfies the following condition:

$$\xi_0 = \frac{\beta/\alpha}{1 + \xi_0^n}. \tag{13}$$

Leakage β' makes the system asymmetric and the new fixed point coordinates (x_0, y_0, z_0) satisfy the following conditions:

$$x_0 = \frac{\beta/\alpha}{1 + z_0^n} + \beta'/\alpha \qquad y_0 = \frac{\beta/\alpha}{1 + x_0^n} \qquad z_0 = \frac{\beta/\alpha}{1 + y_0^n} \tag{14}$$

Linearizing around the fixed point, we can write for the displacements:

$$\dot{\delta x} = -\gamma_x \delta z - \alpha \delta x \qquad \dot{\delta y} = -\gamma_y \delta x - \alpha \delta y \qquad \dot{\delta z} = -\gamma_z \delta y - \alpha \delta z \tag{15}$$

with:

$$\gamma_x = \beta \frac{n z_0^{n-1}}{(1 + z_0)^2} \qquad \gamma_y = \beta \frac{n x_0^{n-1}}{(1 + x_0)^2} \qquad \gamma_z = \beta \frac{n y_0^{n-1}}{(1 + y_0)^2} \tag{16}$$

Rewriting Eq. 15 in matrix form we have:

$$\dot{\boldsymbol{\Delta}} = -\boldsymbol{\Gamma} \cdot \boldsymbol{\Delta} \quad \text{where} \quad \boldsymbol{\Delta} = \begin{pmatrix} \delta_x \\ \delta_y \\ \delta_z \end{pmatrix} \qquad \boldsymbol{\Gamma} = \begin{pmatrix} \alpha & 0 & \gamma_x \\ \gamma_y & \alpha & 0 \\ 0 & \gamma_z & \alpha \end{pmatrix} \qquad (17)$$

The three eigenvalues of $\boldsymbol{\Gamma}$ are $\alpha - \bar{\gamma}e^{i\pi/3}, \alpha + \bar{\gamma}, \alpha - \bar{\gamma}e^{-i\pi/3}$, where $\bar{\gamma} = \sqrt[3]{\gamma_x\gamma_y\gamma_z}$. The fixed point is stable when all the eigenvalues have a positive real part ($\bar{\gamma}/\alpha < 2$). At $\bar{\gamma}/\alpha = 2$ we have an Hopf bifurcation and for $\bar{\gamma}/\alpha > 2$ two eigenvalues acquire a negative real part and a limit cycle arises. We numerically calculated $\bar{\gamma}/\alpha$ as a function of normalized leakage β'/α for the same parameters we used in all the simulations ($\beta = 300$ h^{-1}, $\alpha = 0.75$ h^{-1}, $n = 3$). Results are shown in Supplementary Fig. 5 showing that the Hopf bifurcation occurs for $\beta'/\alpha = 3.24$.

When no leakage is present, β' represents the production of x' induced by green light. As discussed in the main text we estimate an experimental value for $\beta'/\alpha = 107$. This means that in all experiments reported here, light intensity is always strong enough to break limit cycle oscillations if continuously exposed.

Fig. 5 a $\bar{\gamma}$ vs leakage shows that increasing the leakage past a certain threshold the existing limit cycle breaks down and the system does damped oscillations towards the fixed point. **b** The period of the oscillator is affected by the leakage. We plot the curves for the two hill coefficients treated in the manuscript. For $n = 3$ the period is monotonically decreasing in response to leakage increase, suggesting that the period increase in the optorepressilator respect to the repressilator (Fig. 3d main text) is not leakage. In the digital case ($n = \infty$) we see that the leakage breaks the limit cycle for values of $\beta'/\alpha \geq 1$.

6 Quantification of gene expression levels as a function of light intensity

Fig. 6 Samples are DHL708 *E. coli* strain with pNO286-3 plasmid, added with sfGFP light-driven production construct as shown in Fig. 3 of the main text, while control ('ctr') is DHL708 + pNO286-3 + pSR58-0. **a** Protein production rate over green light intensity (same data as Fig. 3b). While being exposed to different green light intensities, all samples were also constantly exposed to $0.74 W/m^2$ red light. Dots are the mean values of experiments repeated on 3 different days. **b** Raw OD600 (top) and sfGFP fluorescence (bottom) data for one of the sfGFP production replicates.

7 Dependence of Phase Response Curves (PRC) on β' and τ

Fig. 7 **a** PRCs of the optorepressilator for $\tau = 2$ h and β' varying logarithmically between 1 h^{-1} and 10^4 h^{-1}. **b** PRCs of the optorepressilator for $\beta' = 80$ h^{-1} and τ varying between 0.02 h and 7.5 h. **c** PRCs of the optorepressilator in the digital approximation ($n = \infty$) for varying β' and τ. The black dashed lines represent the theoretical prediction as described below. The other parameters used in the simulations are $\alpha = 0.75$ h^{-1}, $\beta = 300$ h^{-1}, $n = 3$.

Within the digital approximation ($n \rightarrow \infty$) we can derive approximate expressions for the phase response curve as follows.

Case $\phi > 0$.

When the pulse arrives at a time delay t after the peak, a bump in x' is produced whose rise time is τ while the time t' to decay to the threshold value 1 is given by:

$$\frac{\beta'}{\alpha} \left(1 - e^{-\alpha\tau}\right) e^{-\alpha t'} = 1$$

If x' decays to the threshold after x than the next y peak will be delayed by a time:

$$t + \tau + t' + \frac{T_0}{3} - T_0$$

corresponding to a negative phase shift:

$$\Delta\phi = - \left(\phi + \frac{1}{\alpha T_0} \log \left[\frac{\beta'}{\alpha} \left(e^{\alpha\tau} - 1\right) \right] - \frac{2}{3} \right)$$

The predicted PRC as a negative slope equal to -1 and a intercept that depends on the intensity and duration of the light pulse.

Case $\phi < 0$.

When the pulse arrives before the peak $(t < 0)$ it triggers the decay of y (blue trace) which will reach the threshold 1 after a time t' given by:

$$\frac{\beta}{\alpha} \left(1 - e^{-\alpha(T_0/3+t)}\right) e^{-\alpha t'} = 1$$

When y reaches the threshold, z production will be turned on and quickly reach the threshold for repressing x. From this moment x will start decaying and reach the threshold after a time t'':

$$\frac{\beta}{\alpha} \left(1 - e^{-\alpha(t'+t)}\right) e^{-\alpha t''} = 1$$

Using the previously obtained expression for the period $T_0 = 3\log(\beta/\alpha)/\alpha$ we can finally find that the phase will be positively shifted by:

$$\Delta\phi = \frac{1}{\alpha T_0} \log \left[\frac{\beta}{\alpha} e^{\alpha T_0 \phi} - 2 \right] - \frac{1}{3}$$

This time the PRC is insensitive to the intensity and duration of the light pulse.

These two analytic expressions for the PRC are reported as black dashed lines in Supplementary Fig. 7.

8 Exploring "Arnold surface" at low forcing

Fig. 8 a Arnold surface calculated as in Fig. 6 of main text, with red circles to highlight the values of forcing amplitudes and frequencies used for plots in **b** and **c**. We notice that at a forcing frequency ratios of 1.5 and 1.25, entrainment is achieved only for the higher amplitude values. Interestingly, when moving in between the main plateaus in the Arnold surface we find entrainment at fractional frequency ratios such as $2/3\ f$ at $f/\nu_0 = 1.5$ and $3/2\ f$ at $f/\nu_0 = 0.67$.

9 Correlation of period and amplitude with growth rate

Fig. 9 α values are changed from $1/10$ of the standard value (0.75h^{-1}) to 10 times as much. Amplitude is dimensionless, in units of K. Dots are simulations, the continuous lines are predictions with $n = 3$ or digital approximation $n = \infty$.

10 Strains

Strain	Genotype	Source	Parent
DHL708	MC4100 $\Delta clpPX$	[1]	
MCC0234	DHL708 $\Delta attB :: lacI34$ $P_{\mathrm{cpcG2\text{-}172}}\ BBa\_B0034\ lacI\ (kan)$	this work	DHL708
MCC0233	DHL708 $\Delta attB :: lacI33$ $P_{\mathrm{cpcG2\text{-}172}}\ BBa\_B0033\ lacI\ (kan)$	this work	DHL708
MCC0034	DHL708 $\Delta attB :: gfp34$ $P_{\mathrm{cpcG2\text{-}172}}\ BBa\_B0034\ sfgfp\ (kan)$	this work	DHL708
MCC0033	DHL708 $\Delta attB :: gfp33$ $P_{\mathrm{cpcG2\text{-}172}}\ BBa\_B0033\ sfgfp\ (kan)$	this work	DHL708

Table 1 *Escherichia coli* **strains used in this work.**

Fig. 10 Maps of the original *attB* site and genome insertions. Genome sites correspond to *E. coli* strains: MCC0034 top left, MCC0033 bottom left, MCC0234 top right, MCC0233 bottom right. All maps are created with SnapGene.

11 Plasmids

Plasmid	Description	Source	Parent
pLPT234	core repressilator components and reporters	[2]	
pLPT145	repressors' sponge	[1]	
pNO286-3	light sensor and PCB enzymes	[3]	
pSR58.6	CcaR, light-driven sfGFP production (RBS BBa_B0034)	[4]	
pSR58.b33	CcaR, light-driven sfGFP production (RBS BBa_B0033)	this work	pSR58.6
pSR58-0	CcaR, no $P_{cpcG2\text{-}172}$ nor sfGFP	this work	pSR58.6
pSpongeROG.b34	light-driven LacI production (RBS BBa_B0034), repressors's sponge, CcaR	this work	pSR58.6 (backbone), pLPT145 (sponge), pLPT234 (*lacI*)
pSpongeROG.b33	light-driven LacI production (RBS BBa_B0033), repressors's sponge, CcaR	this work	pSR58.6 (backbone), pLPT145 (sponge), pLPT234 (*lacI*)
pSpongeROG0	repressors's sponge, CcaR	this work	pSR58.6 (backbone), pLPT145 (sponge)
pKD46-sfGFP.b34	genome insertion of light-driven sfGFP cassette	this work	pKD46 (backbone), pSR58.6
pKD46-sfGFP.b33	genome insertion of light-driven sfGFP cassette	this work	pKD46 (backbone), pSR58.b33
pKD46-lacI.b34	genome insertion of light-driven lacI cassette	this work	pKD46 (backbone), pSpongeROG.b34
pKD46-lacI.b33	genome insertion of light-driven lacI cassette	this work	pKD46 (backbone), pSpongeROG.b33

Table 2 Plasmids

Fig. 11 Plasmid maps. All maps are created with SnapGene.

12 Antibiotic concentrations

Antibiotic	working concentration
Streptomycin	50 μg/ml
Ampicillin	100 μg/ml
Kanamycin	50 μg/ml
Chloramphenicol	20 μg/ml
Spectinomycin	100 μg/ml

Table 3 Antibiotic concentrations

13 Microscope setup

Fig. 12 Microscope setup used for mothermachine experiments.

14 Description of Supplemental Videos

The snapshots of CFP fluorescence were acquired every 9 minutes and the videos are played at 32 frames/s. The presence of a green square over the image indicates that at that time point the bacteria are exposed to green light stimuli provided by the Thorlabs LED M530L4. The fluorescence of each mother cell and the mean fluorescence of all mother cells are plotted in the main text respectively in Fig. 4b for Supplementary Video 1 and in Fig. 5e for Supplementary Video 2.

References

[1] Potvin-Trottier, L., Lord, N.D., Vinnicombe, G., Paulsson, J.: Synchronous long-term oscillations in a synthetic gene circuit. Nature Letters **538**, 514–517 (2016)

[2] Riglar, D.T., Richmond, D.L., Potvin-Trottier, L., Verdegaal, A.A., Naydich, A.D., Bakshi, S., Leoncini, E., Lyon, L.G., Paulsson, J., Silver, P.A.: Bacterial variability in the mammalian gut captured by a single-cell synthetic oscillator. Nature Communications **10**(1), 1–12 (2019) https://doi.org/10.1038/s41467-019-12638-z

[3] Ong, N.T., Tabor, J.J.: A miniaturized escherichia coli green light sensor with high dynamic range. ChemBioChem **19**(12), 1255–1258 (2018)

[4] Schmidl, S.R., Sheth, R.U., Wu, A., Tabor, J.J.: Refactoring and optimization of light-switchable escherichia coli two-component systems. ACS Synthetic Biology **3**(11), 820–831 (2014)