A high-density diffuse optical tomography dataset of naturalistic viewing

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Running title: HD-DOT movie dataset

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42   **Abstract**

Traditional laboratory tasks offer tight experimental control but lack the richness of our
everyday human experience. As a result many cognitive neuroscientists have been
motivated to adopt experimental paradigms that are more natural, such as stories and
movies. Here we describe data collected from 58 healthy adult participants (aged 18–76
years) who viewed 10 minutes of a movie (*The Good, the Bad, and the Ugly*, 1966).
Most (36) participants viewed the clip more than once, resulting in 106 sessions of data.
Cortical responses were mapped using high-density diffuse optical tomography (first-
through fourth nearest neighbor separations of 1.3, 3.0, 3.9, and 4.7 cm), covering large
portions of superficial occipital, temporal, parietal, and frontal lobes. Consistency of
measured activity across subjects was quantified using intersubject correlation analysis.
Data are provided in both channel format (SNIRF) and projected to standard space
(NIfTI), using an atlas-based light model. These data are suitable for methods
exploration as well as investigating a wide variety of cognitive phenomena.
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Background & Summary

Most cognitive neuroscientists are interested in how human brains navigate the real
world. To do so, we frequently create tightly-controlled laboratory paradigms intended to
isolate one or more aspects of sensory or cognitive processing. We hope that the
findings from these purposefully artificial experiments will generalize to real-world
scenarios. However, is such an assumption justified? To answer this question, cognitive
neuroscience has been increasingly moving towards the use of naturalistic stimuli (Zaki
and Ochsner, 2009; Sonkusare et al., 2019; Nastase et al., 2020; Finn et al., 2022).
For over 20 years, researchers using fMRI have explored the use of movies to
provide rich stimulation for research participants including newborns , children
(Richardson et al., 2018; Yates et al., 2021; Tansey et al., 2023), healthy adults (Zacks
et al., 2001; Hasson et al., 2004; Naci et al., 2014; Chen et al., 2017; Aliko et al., 2020;
Caldinelli and Cusack, 2022), and numerous other populations (Loiotile et al., 2019;
Lyons et al., 2020; Musz et al., 2022; Yao et al., 2022). Although not completely
naturalistic, movies convey complex auditory and visual information covering a range of
sensory, cognitive, and linguistic domains. Movies therefore provide researchers the
opportunity to study processing that more closely mimics everyday experience than
standard laboratory tasks. Additionally, the ability to concurrently address multiple
domains of sensory and cognitive processing may make movies a more efficient way to
collect data than traditional cognitive psychology paradigms. For example, 10 minutes
of movie data collection might replace 30 minutes of domain-specific data collection
(e.g., 10 minutes of an auditory task, 10 minutes of a visual task, 10 minutes of a
language task).
Optical neuroimaging, particularly functional near infrared spectroscopy (fNIRS),
offers many advantages for studying human brain function. First, it is acoustically silent,
avoiding the auditory confounds present in fMRI (Peelle, 2014). Second, implanted
medical devices are not contraindicated, meaning optical imaging can be used on
people with implanted medical devices, such as cochlear implants (Saliba et al., 2016;
Sherafati et al., 2022) or implanted electrodes used for deep brain stimulation
(Eggebrecht et al., 2014). Finally, fNIRS facilitates real-world applications including
imaging during face-to-face interaction (Hirsch et al., 2020). These advantages make
fNIRS well suited for studying cognition in context (Thomas, 2023) that includes social
interaction (Dingemanse et al., 2023).
Traditionally, drawbacks associated with fNIRS include limited coverage of the
cortex, uneven sensitivity over the field of view, and lack of depth information necessary
for removing superficial (i.e., non-brain) hemodynamic components. These challenges
motivated the development of high-density diffuse optical tomography (HD-DOT), in
which a lattice of closely-spaced sources and detectors provides homogenous
sensitivity and spatial resolution comparable to that obtained in fMRI (**Figure 1**)
(Eggebrecht et al., 2014).
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Figure 1. a) Illustration of HD-DOT cap and optode arrangement (see Eggebrecht et al., 2014 for details). **b)** Illustration of field of view in the reconstructed images.

Here, we present data collected using custom high-density optical tomography during movie-viewing. Although the use of movies in HD-DOT has been previously explored (Fishell et al., 2019), our hope is that by making the current data available we will facilitate methodological and theoretical advances related to naturalistic stimulation. These include identification of quality control metrics, how to best handle estimated motion, and optimal methods for modeling quasi-continuous variables.

Method

Participants
Data from 58 participants are included in the data set, ranging in age from 18–76 years (M = 23; F = 35; mean age = 31); self-reported handedness (right = 55, left = 2, ambidextrous = 1). Forty nine of the participants reported English as the first language they learned. Participants were recruited from the Washington University in Saint Louis community. In addition, participants reported to have normal vision and hearing and no known history of neurological disorders. All participants gave written informed consent prior to the experiment session, which was approved by and carried out in accordance with the Human Research Protection Office at Washington University.

Stimulus
The stimulus was a 10-minute clip taken from *The Good, the Bad, and the Ugly* (1966), a movie previously used in fMRI (Hasson et al., 2004) and HD-DOT (Fishell et al., 2019). All participants viewed between 16 minutes and 48 sec and 26 minutes 48 sec. A subset of the participants viewed a longer clip; in this case, their data were truncated to 10 minutes so that all participants had the same amount of data covering an identical portion of the movie. Copyright restrictions preclude openly sharing the stimulus but guidance is available on request from the corresponding author. We did not

systematically document whether participants had previously viewed the selected clip;
anecdotally, most participants reported being unfamiliar with the movie.
The same movie clip was used in several projects between 2012–2022 and thus
was presented along with various other tasks, including auditory, visual, motor,
language, and collection of resting state data. Analyses including 7 of these participants
have been published previously (Fishell et al., 2019) but none of the data is included in
a public data set.

Procedure
Participants were seated on a comfortable chair in an acoustically isolated room facing
an LCD screen located 76 cm from them, at approximately eye level, which displayed
the movie. The soundtrack was presented through two speakers located approximately
150 cm away at about ± 21° from the subjects' ears. The sound level was approximately
65 dBA but not calibrated. The HD-DOT cap was fitted to the subject's head to
maximize optode-scalp coupling, assessed via real-time coupling coefficient readouts
using in-house software. The movie was presented using Psychophysics Toolbox 3
(Brainard, 1997) (RRID:SCR_002881) in MATLAB.

Data acquisition
Data was acquired using two different continuous wave HD-DOT caps. The first cap had
96 sources and 92 detectors (LED) (shining 750 nm and 850 nm near-infrared light)
(Eggebrecht et al., 2014) and was used in 9 (of total 58) participants. The second cap
was built by attaching an additional pad on top of the previous cap and had 128 sources
and 125 detectors (Laser diode) (shining 685 nm and 830 nm near-infrared light) and
was used in the remaining 49 participants. Source-detector pairs were arranged on both
caps to enable first- through fourth nearest neighbor separations of 1.3, 3.0, 3.9, and
4.7 cm, respectively. Our in-house software controlled temporal, frequency, and spatial
encoding patterns which achieved an overall framerate of 10 Hz.
Full measurement sets are available in the raw data formats (NeuroDOT and
snirf). In order to make the analyses in this paper consistent, we have removed all the
measurements from the additional motor pad in 49 participants that were scanned using
the bigger cap to contain the same 96 sources and 92 detectors as the other subjects in
the preprocessed data formats (nii and BIDS) and all the analyses presented in this
paper.

Data processing
Data processing is schematically illustrated in **Figure 2**. Data preprocessing was done
using the NeuroDOT toolbox (https://www.nitrc.org/projects/neurodot) based on the
principles of modeling light emission, diffusion, and detection through the head
(Eggebrecht and Culver, 2019; Sherafati et al., 2022). Data processing steps included
taking the log-mean ratio of the light levels for each time-point and the temporal mean
across the run (as a baseline value). This step was followed by excluding any source-
detector measurement that had a temporal standard deviation of 7.5% in the least-noisy
60 sec (lowest mean GVTD; Sherafati et al., 2020) of each run or higher to exclude any
noisy measurements due to poor optode-scalp coupling or movement. Due to low SNR,
we did not use the measurements beyond second nearest neighbors. The

measurements were then high-pass filtered (0.02 Hz cutoff) to remove low-frequency
drift. We then estimated and regressed the global superficial signal as the average of all
first nearest neighbor measurements (1.3 cm source-detector pair separation) (Gregg et
al., 2010). Following that, data were low-pass filtered to 0.5 Hz cutoff to remove cardiac
oscillations. These frequencies were chosen in all previous studies that were published
using the existing HD-DOT devices and are consistent with best practices (Yücel et al.,
2021). Data were then down-sampled from 10 to 1 Hz and then used for image
reconstruction.
We then computed a forward model of light propagation based on the two
wavelengths used for each device on an anatomical atlas including the non-uniform
tissue structures: scalp, skull, CSF, gray matter, and white matter (Ferradal et al.,
2014). The resulting sensitivity matrix was then inverted for calculating the relative
changes in absorption at the two wavelengths via reconstruction using Tikhonov
regularization and spatially variant regularization (Eggebrecht et al., 2014). Relative
changes in oxygenated, deoxygenated, and total hemoglobin (ΔHbO, HbR, ΔHbT) were
then computed using the absorption and extinction coefficients of oxygenated and
deoxygenated hemoglobin at the two wavelengths. We resampled all data to a $3 \times 3 \times 3$
mm standard atlas using a linear affine transformation.

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The preprocessed data were then
converted to the NIfTI file format for
analysis and sharing purposes.
Intersubject correlation analysis was
performed using the automatic analysis
(aa) environment (Cusack et al., 2015),
version 5.8. Additionally, the *ndot2snirf*
function in NeuroDOT was used to
convert the raw data to SNIRF file
format followed by *snirf2bids* function to
generate other necessary metadata files
to satisfy the BIDS specification for
NIRS (Gorgolewski et al., 2016; Tucker
et al., 2023). In addition to using these
standard functions, the NIfTI files were
cropped to align with the actual start and
end points of the movie stimulus.

204   **Data Records**

The data records are organized
following the Brain Imaging Data
Structure (BIDS standard (Gorgolewski
et al., 2016) and available as dataset
ds004569 on OpenNeuro (Markiewicz et
al., 2021), and listed on OpenfNIRS.org.

211   **Technical Validation**

Data quality
To quantify data quality across sessions
we focused on two measures intended
to capture effects of participant motion
and light levels (**Figure 3**). Because we
do not have objective measures of
motion (e.g., photometry or
accelerometers), we rely on a signal-
based proxy for motion: global variance
of temporal derivatives (GVTD)
(Sherafati et al., 2020). GVTD is
conceptually similar to the DVARS
measure sometimes used in fMRI
(Smyser et al., 2011; Power et al., 2012).

Figure 2. Schematic of data processing and file formats. The data are provided in three different formats: SNIRF, NeuroDOT, and NIfTI.

We used the heartbeat (pulse) signal-to-noise ratio (SNR) as an indicator of detecting physiological signal in the data. The pulse SNR was calculated as the proportion of the pulse power (based on the peak FFT magnitudes in the 0.5–2 Hz window) divided by a noise floor (based on the FFT magnitudes in the 0.5–1 Hz window).

Figure 3. Quality control measures. **a)** Mean light levels over the cap for a sample participant (850 nm light). **b)** *Top:* example temporal derivative time traces from source detector distances between 1–19 mm, 20–29 mm, and 30–40 mm respectively, for 850 nm light in the same sample participant; *Bottom:* GVTD over the same time period. **c)** Scatter plot of GVTD (proxy for motion) and pulse levels for all sessions.

Intersubject correlation analyses

In an intersubject correlation analysis, the similarity of time courses is computed for the same voxel in each pair of participants; averaging these values provides an average intersubject correlation value for every voxel of the brain (Nastase et al., 2019). Numerous studies have used intersubject correlation analysis to identify regions of the brain which show similar patterns of activity across a group of participants. For movie viewing, these values are typically higher in sensory regions (e.g, visual cortex and auditory cortex) than regions associated with complex linguistic or executive processing (Hasson et al., 2004; Visconti di Oleggio Castello et al., 2020). One benefit of intersubject correlation analysis is that it is sensitive to shifts in the timing of activity across participants. Thus, demonstrating reasonable intersubject correlation values in sensory regions suggests the time courses across participants are correctly temporally aligned.

As part of our technical validation, we therefore performed an intersubject correlation analysis (**Figure 4a**). Because not all participants had multiple sessions of movie data, we restricted our analysis to the session with the highest pulse SNR from each participant. The signal average was subtracted from each frame and a Pearson

correlation coefficient was then computed voxel-wise using the corrected data for all
pairs of subjects. We see the highest values in auditory and visual cortices, broadly
consistent with prior studies in both fMRI (Hasson et al., 2004) and HD-DOT (Fishell et
al., 2019).
We then placed participants into one of three groups based on pulse amplitude
measured in the optical signal (low group: 3.0 < pulse ≤ 6.0; med: 6.0 < pulse ≤ 14.5;
high: 14.5 < pulse < 25.5). As shown in **Figure 4b**, we observed that r values were
notably higher in subjects in the high pulse amplitude group compared to those in the
medium and low groups, supporting our use of pulse amplitude as a quality control
measure.
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Figure 4. Intersubject correlation analysis. **a)** Correlation map shows the average pairwise correlation across all subjects. Maximum r-values are observed in sensory areas. The SNR in these subjects, as quantified by pulse amplitude, ranged from approximately 3 to 25. **b)** A histogram of pulse values, and used to separate subjects into low (red), medium (blue), and high (green) SNR groups. **c)** Correlation maps obtained for subjects grouped by SNR. High correlations extend beyond sensory areas in the highest SNR group.

262   **Code Availability**

263   Code used for technical validation is available from http://github.com/jpeelle/GBUDOT.

Acknowledgments

This work was supported by R01 DC019507, R21 DC016086, R21 DC015884, R01 MH122751, K01 MH103594, R21 NS098020, and T32 EB014855 from the US National Institutes of Health. We thank Tessa G. George, Kelsey T. King, Karla M. Bergonzi, and Tracy M. Burns-Yocum for assistance with data collection.

Author Contributions

J.E.P. conceived of the data sharing effort. A.F., A.S., A.B., M.M., and C.H.L. collected the data. E.S., A.B., and A.S. oversaw data conversion and organization. A.B., A.S., M.S.J. completed preprocessing and quality control analyses. M.S.J. conducted the intersubject correlation analyses. The manuscript was drafted by J.E.P., A.S., A.B., and M.S.J., and critically reviewed by all authors. J.E.P., J.P.C., A.T.E., and T.H. obtained funding.

Competing Interests

The authors declare no competing interests.

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