Title
Shared and diverging neural dynamics underlying false and veridical perception

Short title
Neural dynamics underlying false and veridical percepts

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Abstract

We often mistake visual noise for meaningful images, particularly when we strongly expect to see something. For instance, a cat owner might in a poorly lit room mistake a shadowy figure for a cat, due to their expectation to see one. These false percepts can sometimes be as convincing as veridical perception, leading to perceptual judgements of equal confidence. How might seemingly equivalent perceptual judgements occur in the face of such different sensory inputs? One possibility is that while false and veridical percepts are generated by different early sensory processes, subsequent neural mechanisms driving perceptual confidence are identical. To test this possibility, we used MEG to examine the neural mechanisms underlying veridical and false perception with high temporal precision. Participants performed a visual discrimination task requiring them to detect gratings with different orientations under high levels of sensory noise, while on 50% of trials no gratings were presented (noise-only trials). On a subset of noise-only trials, participants reported seeing a grating with high confidence, dubbed here false percepts. We found that high alpha/low beta [11-14Hz] power was increased just before falsely perceiving a grating in noise, but not before veridical percepts, potentially reflecting enhanced reliance on top-down signalling during false percepts. From 250ms post-stimulus, a converging neural signal reflecting perceptual confidence emerged for both absence and presence trials, reflecting an early final common pathway for both veridical and false perceptual inference.

Significance statement

The neural mechanisms underlying false percepts are likely different from those that underlie veridical perception, as the former are generated endogenously, whereas the latter are the result of an external stimulus. Yet, false percepts often get confused for veridical perception, suggesting a converging mechanism. This study explores when the neural mechanisms of false and veridical perception diverge and converge. We found that false, but not veridical, percepts were preceded by increased high alpha/low beta [11-14 Hz] power, possibly reflecting a reliance on endogenous signals. From 250ms post-stimulus onwards, there was a converging neural signal reflecting confidence in the percept, shared by veridical and false percepts.

Introduction

When we try to make sense of our noisy visual surroundings, we sometimes mistake our own internally generated signals for externally caused sensations. For example, a cat owner may have such a strong expectation to see their pet that they misperceive a blurry flash in their visual periphery as their cat. However, despite these false perceptual experiences relying on different neural signals than veridical percepts, they sometimes appear to be just as real. This poses a conundrum. On the one hand the neural mechanisms that underlie veridical and false perception are distinct, as the former involves a sensory feedforward signal caused by an external stimulus, whereas the latter arises from internally generated signals. However, ultimately, they result in similar perceptual judgements, suggesting a final common pathway onto which the neural processes converge. When and how these neural mechanisms diverge and converge remains unclear. Here, we explore the unique and converging neural mechanisms underlying veridical and false perception using MEG.

Previous studies have explored the role of pre-stimulus oscillations in biasing perception. A consistent finding is that a decrease in alpha power leads to increased hit rates on stimulus present trials by inducing a more liberal detection threshold, while not affecting sensitivity (Achim et al., 2013; Benwell et al., 2017; Boncompte et al., 2016; Brüers & VanRullen, 2018; Chaumon & Busch, 2014; Ergenoglu et al., 2004; Iemi et al., 2017; Iemi & Busch, 2018; Mathewson et al., 2014; Samaha et al., 2017, 2020; Van Dijk et al., 2008). Mechanistically, this could be achieved by increasing neuronal excitability (Samaha et al., 2017, 2020). The relationship between alpha power and false percepts remains less well understood. For example, illusory perception during double flash illusions has been linked to both lower alpha power (Lange et al., 2013) as well as increased, rather than lower, beta power (Keil et al., 2014). In sum, how alpha and beta oscillations exactly relate to false percepts remains inconclusive.

A second body of work has linked alpha and beta to top-down cognitive processes. Although classically linked to the motor domain, various studies have found that top-down processes like visual search and attention lead to increased beta power (Buschman & Miller, 2007, 2009; Engel & Fries, 2010; Pesaran et al., 2008). Importantly, higher beta power has been linked to interpreting ambiguous stimuli in the language (Iversen et al., 2009) and visual domains (Hipp et al., 2011; Okazaki et al., 2008). Mental imagery, a cognitive process arguably exclusively reliant on top-down mechanisms, has also been shown to lead to increased alpha and beta power (Bartsch et al., 2015; Villena-González et al., 2018). Finally, prediction – arguably a fundamental mechanism of the brain (Friston, 2018) – has been suggested to be implemented through alpha and beta oscillations (Bastos et al., 2012; Engel et al., 2001). Empirical evidence for this has emerged in recent years tying enhanced high alpha/low beta power to predictions (Auksztulewicz et al., 2017; Fujioka et al., 2012; Sherman et al., 2016; Turner et al., 2023). Finally, a study in monkeys linked an increase in beta power to processing predictable information, further finding that beta oscillations originated from cortical layers typically associated with feedback signalling, and exerted a causal influence on lower-level sensory regions (Bastos et al., 2020). In sum, alpha and beta oscillations are implicated in top-down mechanisms like imagination and prediction. However, it remains unclear to what extent these oscillations contribute to false perception, and at what point the neural mechanisms of veridical and false perception converge.

To test this, the current study investigated the role of alpha and beta oscillations in false perception during a difficult perceptual discrimination task, using time frequency and decoding analyses to explore the oscillatory dynamics and converging neural signals underlying false and veridical perception. To preview, we find that false, but not veridical percepts were associated with an increase in pre-stimulus high alpha/low beta (11-14Hz) power, possibly reflecting endogenous feedback signals. Furthermore, decoding analyses revealed a post-stimulus neural code reflecting perceptual judgements of stimulus presence that was shared between veridical and false perception.

Methods

Ethics statement

This study was approved by the University College London Research Ethics Committee (R13061/RE002) and conducted according to the principles of the Declaration of Helsinki. All participants gave written informed consent prior to participation and received monetary compensation (£7.50 an hour for behavioural training, £10 an hour for MEG).

Participants

Twenty-five healthy human volunteers with normal or corrected-to-normal vision participated in the MEG experiment. Two participants were excluded due to missing trigger data. The final sample consisted of 23 participants (22 female; age 25 ± 4 years; mean ± SD).

Stimuli

Grayscale luminance-defined sinusoidal grating stimuli were generated using MATLAB (MathWorks, Natick, Massachusetts, United States of America, RRID:SCR_001622) and the Psychophysics Toolbox (Brainard, 1997). During the behavioural session, the stimuli were presented on a PC (1024 × 768 screen resolution, 60-Hz refresh rate). During the MEG recording session, stimuli were projected onto a screen in front of the participant (1920 × 1200 screen resolution, 60-Hz refresh rate). On grating-present trials (50%), auditory cues were followed by a grating after a 750ms delay (0.5-cpd spatial frequency, 33ms duration), displayed in an annulus (outer diameter: 10° of visual angle, inner diameter: 1°, contrast decreasing linearly to 0 over 0.7° at the inner and outer edges), surrounding a fixation bull's eye (0.7° diameter). These stimuli were combined with one of 4 noise patches, which resulted in a 4% contrast grating embedded in 20% contrast noise during the MEG session. On noise-only trials, one of the 4 noise patches was presented on its own. Noise patches were created by smoothing pixel-by-pixel Gaussian noise with a Gaussian smoothing filter, ensuring that the spatial frequency of the noise matched the gratings (Wyart et al., 2012). This was done to ensure that the noise patches and gratings had similar low-level properties, increasing the likelihood of false percepts (Pajani et al., 2015). To avoid including noise patches which contained grating-like orientation signals by chance, 1000 noise patches were processed through a bank of Gabor filters with varying preferred orientations. Only noise patches with low (2%) signal energy for all orientations were selected to be included in the present experiment. The resulting four noise patches were used for all trials throughout the experiment, in a counterbalanced manner, ensuring that reported false percepts could only be triggered by internal mechanisms (Haarsma et al., 2023; Pajani et al., 2015). During the practice session on the first day, the contrast of the gratings was initially high (80%), gradually decreasing to 4% towards the end of the practice. The central fixation bull's-eye was present throughout the trial, as well as during the intertrial interval (ITI; randomly varied between 1000 and 1200ms).

Experimental procedure

Participant were required to perform a visual perceptual discrimination task. Trials consisted of an auditory expectation cue, followed by a grating stimulus embedded in noise on 50% of trials (750ms stimulus onset asynchrony (SOA) between cue and grating). The auditory cue (high or a low tone) predicted the orientation of the grating stimulus (45° or 135°) on grating-present trials. On these grating-present trials, a grating with the orientation predicted by the auditory cue was presented embedded in noise, while on noise-only trials (50%) only a noise

patch was presented. The stimulus was presented for 33ms. After the stimulus disappeared, the orientation response prompt appeared, consisting of a left and right pointing arrow on either side of the fixation dot (location was counterbalanced). Participants were required to select the arrow corresponding to their answer (left arrow for anti-clockwise, or 135°, right arrow for clockwise, or 45°; 1s response window) through a button press with their right hand, using either a button box in the MEG, or a keyboard during behavioural training. Subsequently the letters "CONF?" appeared on the screen probing participants to indicate their confidence that they had seen a grating (1 = I did not see a grating, 2 = I may have seen a grating, 3 = I probably saw a grating, 4 = I am sure I saw a grating), using 1 of 4 buttons with their left hand (1.25s response window). It is worth highlighting here that confidence here reflected participants' belief that a grating was present, not their confidence in their orientation report. It therefore reflects a perceptual awareness scale response (Sandberg & Overgaard, 2015).

On the first day of testing, participants took part in a behavioural practice session. The practice consisted of an instruction phase with 7 blocks of 16 trials where the task was made progressively more difficult, whilst verbal and written instructions were provided. During these practice runs, the auditory cues predicted the orientation of the grating stimulus with 100% validity (45° or 135°; no noise-only trials). After the completion of the instructions, the participants completed 4 runs of 128 trials each, separated into 2 blocks of 64 trials each. In the first 2 runs the expectation cues were 100% valid, to ensure participants learnt the association, whilst in the final 2 runs the cues were 75% valid (i.e., the grating had an unexpected orientation on 25% of trials), to test whether participants might have adopted a response bias. Grating contrast decreased over the 4 runs, specifically the contrast levels were 7.5, 6, 5, and 4%, while the contrast of the noise patches remained constant at 20%. No noise-only trials were presented on day 1. On the second day, participants performed the same task during the MEG recording. During this session, 8 runs were completed, each consisting of 64 trials. This time the grating contrast was fixed at 4% on grating-present trials, and on 50% of the trials the gratings were omitted and only noise patches were presented, resulting in noise-only trials (Fig. 1a). On grating-present trials the cues always predicted the orientation of the grating with 100% validity (Fig. 1b). On noise-only trials the cue was by definition invalid, since no grating was presented. After each run a localiser run followed where gratings oriented either 45° or 135° were presented while participants performed a distracting fixation dimming task. The purpose of this localiser run was to uncover an orientation-specific MEG signal, which will not feature in the present paper as we were not able to uncover a significant orientation-specific signal evoked by the noisy stimuli presented in the current experiment. This analysis did reveal orientation-specific activity during the response window, which will be reported in detail elsewhere. Each run lasted ~8 minutes, totalling ~64 minutes.

Pre-processing of MEG data

MEG was recorded continuously at 600 samples/second, using a whole-head 273 channel axial gradiometer system (CTF Omega, VSM MedTech), while participants sat upright. A photodiode was used to measure the onset of the visual stimuli through the presentation of a small white square in the bottom-right corner of the screen on both localiser trials as well as main experiment trials. This was done to ensure that the trials were aligned exactly to stimulus presentation. Note that the white square was not visible to participants, as it was covered by the electrode. The first experimental run (out of 8) for each subject was removed, leaving 7 runs for analyses. Trials were segmented 3000ms pre-stimulus and 3000ms post-stimulus. Movement and eye-blink artefacts were manually selected and inspected before

being rejected from the data. Independent component analyses were applied to the complete dataset to identify components that reflect eye-blinks as well as cardiac related signals, which were manually inspected and removed from the data for each subject.

ERF analyses

ERF analyses were conducted for exploratory reasons. We tested for differences in ERF amplitude for high and low confidence trials. Cluster-based analyses where then conducted on the sensor-level using Monte-Carlo permutation tests (N=10000), at a significance threshold of $p<.05$ for the initial threshold for determining a significant difference in ERF as well as for determining significant clusters. ERFs were computed separately for high and low confidence trials, for both grating-present and noise-only trials.

Frequency analyses

Frequency power was estimated across all MEG channels from 2000ms pre-stimulus to 2000ms post-stimulus in steps of 50ms, for the frequencies 2Hz to 30Hz with steps of 1Hz, using Morlet wavelets (width=7). To test for pre-stimulus changes in alpha and beta power, we used cluster-based-permutation tests with 10000 iterations, at a significance threshold of $p < 0.05$, while averaging over the alpha band (8-12Hz) or the beta band (12-20Hz). For pre-stimulus effects we tested the time window from the onset of the cue to the onset of the stimulus, i.e. -750ms to 0ms. For post-stimulus effects the time window of interest ranged from 0ms to 1000ms. We conducted additional exploratory analyses that included the full pre-stimulus time-window -2000ms and full post-stimulus time-window. Note that these time windows include the onset of the auditory stimulus (-750ms) and the orientation response cues (1000ms). We furthermore repeated the analyses for each frequency between 8 and 20 Hz with steps of 1Hz to estimate which specific frequencies drove the effects.

Decoding analyses

We decoded participants' confidence in stimulus presence from the MEG signal using a two-class linear discriminant analysis (LDA) (Mostert et al. 2015). For these purposes, participants' confidence in stimulus presence was transformed into a binary variable reflecting whether they reported higher or lower than average confidence on a specific trial. The 273 MEG channels were used as features. The decoding used a leave-one out procedure, where all blocks except one served as the training data to decode the remaining block. This procedure was repeated for all blocks. Time points were averaged across a moving time window of 17ms, with steps of 3ms. The covariance matrix is taken into account in the decoder as recommended in previous studies to address correlations between neighbouring MEG sensors (Brouwer & Heeger, 2009; Mostert et al., 2015). For details on the implementation of the decoder, see Mostert et al. 2015. Cluster-based analyses were conducted on both the temporal generalisation matrix as well as its diagonal. In the first step of the permutation, clusters were defined by adjacent points that crossed a significance threshold of $p <.05$. The number of permutations was limited to 1000 due to the large sample space for the temporal generalisation matrix, but was 10000 for the diagonal. A cluster in the true data was considered significant if $p<.05$ based on the null distribution generated by the permutations. The time window of interest initially was -1000ms to 2000ms relative to stimulus onset. Follow-up analyses were almost exclusively conducted on the post-stimulus time window (-100ms to 2000ms), as this showed the only significant effect of confidence decoding. These follow-up analyses involved cross-decoding between noise-only and grating-present trials, to

explore whether they shared a neural code for perceptual confidence. Furthermore, we performed control analyses where we balanced the number of trials in the high and low perceptual confidence conditions by subsampling to the condition with the fewest trials, to ensure that the effects were not driven by an overrepresentation of a single condition.

Source localisation

To visualise the source of the confidence decoding we performed source localisation analyses. We did not collect individual anatomical MRI scans for our subjects, instead, a template MRI and default head and source models as present in the Fieldtrip toolbox (www.fieldtriptoolbox.org) were used (see below) (Oostenveld et al., 2011). Previous studies have demonstrated that little anatomical specificity is lost using a group-based template approach (Holliday et al., 2003).

The spatial pattern that underlies classification in a linear discrimination analysis is driven by the difference in magnetic fields between the two conditions on which the decoding is based. Therefore, one can visualise the source of a decoder by estimating the sources of the two different conditions, and compute the difference (Haufe et al., 2014). For our purposes we computed the absolute difference within the 1000ms to 2000ms time window (where decoding was strongest), divided by the source map of the low confidence condition, thereby estimating percentage signal change. Taking the absolute difference will visualise which source signals are involved in perceptual confidence, without making assumptions about the sign of the signal.

We also performed source localisation on the frequency analyses. Here, there was a direct translation from the univariate effects to the underlying source map, as they seek to refute the same null-hypothesis. We therefore computed cluster-based statistics on the -750ms to 0ms time window for the difference in 13Hz (+- 1.5Hz) power between high and low confidence false percept conditions in source space. The same parameters were used as on the sensor level (10000 permutations, cluster-defining threshold: p=.05, cluster-level threshold: p=.05).

For both the frequency and decoding source localisation, we used the default forward and source models from the Fieldtrip toolbox which were then warped to participants' specific fiducials based on the MEG sensors. The spatial filter was computed for the time windows of interest in the averaged data, which was subsequently applied separately to the two conditions of interest (high and low confidence trials). Source localisation was then computed for the two conditions of interests. For the confidence decoding a percentage absolute signal change was computed in source space, whereas for the frequency analyses t-maps were visualised for significant clusters.

Behavioural analyses

We tested participants' accuracy scores, as well as the relationship between accuracy and confidence in stimulus presence. We further tested whether participants were significantly biased by the auditory cues on noise-only trials, and performed post-hoc tests to see whether these effects were driven by cue awareness. All tests were conducted within-subject and two-sided. Statistics were conducted in JASP (JASP team, 2023).

Results

Participants experienced false percepts that were independent of perceptual expectation cues

Participants accurately identified the grating orientation on grating-present trials more often than expected by chance (mean accuracy=0.66, SD=.12, T{24}=6.5, *p*<.001). Furthermore, they were more accurate when they were confident that they had seen a grating (i.e., higher than average confidence across trials) than when they were not (high: mean=.70, SD=.13; low: mean=.59, SD=.11; paired t-test) (T{24}=6.76, *p*<.001) (Fig. 1c), demonstrating that they were able to perform the task and used the confidence ratings in a meaningful way. It is worth repeating that here participants reported their confidence in having seen a grating, rather than confidence in their orientation report, and thus effectively reflected a perceptual awareness response (Sandberg & Overgaard, 2015). Participants were slightly more confident on grating-present trials (mean confidence =2.29, SD=.64, on a scale of 1-4) than noise-only trials (mean=2.25, SD=.64) (T{24}=2.28, *p*=.031). Upon debriefing, all participants but one underestimated the frequency of noise-only trials, believing on average that .18 (SD=.16) of trials contained just noise, while the true proportion was .50 (Fig. 1d). Strikingly, participants reported perceiving a grating with high confidence (3 out of 4 or higher) on 35% of noise-only trials (Fig. 1f). The perceptual expectation cues significantly biased which orientation participants perceived on noise-only trials (0.55 false percepts congruent with the cue, chance level is .50, T{24}=2.53, *p* =.018). This effect was driven by the individuals who became aware of the meaning of the cues (N = 7 out of 25; Fig. 1e), potentially reflecting a response bias. Indeed, those aware of the cue had significantly stronger effects of the cue (T{24}=4.14, *p*<.001). High confidence false percepts were not more affected by the cues than low confidence percepts, i.e. guesses (T{23}= 1.18, *p*=.24). In sum, these results indicate that participants regularly had false grating percepts, but that these were hardly, if at all, affected by the predictive cues. This is highly consistent with a previous study using the same experimental paradigm (Haarsma et al., 2023).

False percepts were preceded by an increase in pre-stimulus beta power

We tested whether changes in power in the alpha and beta bands preceded high confidence false percepts, that is, trials on which participants indicated high confidence in having seen a grating in the absence of one. We tested for an interaction using a two-way repeated measures ANOVA with confidence and stimulus presence as two-level factors within the -750ms to 0ms time window. This is the time window from the auditory cue, signalling the orientation of an upcoming grating, to the onset of the stimulus. There was a significant interaction in the beta band (12-20Hz) (-650ms to -50ms, *p*=.0039). This interaction between stimulus presence and confidence on beta power remained significant when extending the time-window to -2000ms to 0ms (-650ms to -50ms, *p*=.018), showing that the effect was specific to the post auditory cue period (which started at -750ms). The effect was not significant in the alpha band (8-12Hz, -650ms to 0ms, *p*=.0939). We conducted post-hoc analyses to estimate the exact frequencies that drove these effects by repeating the analyses in steps of 1Hz. This revealed the effect started in the high alpha band (11Hz, -700ms to -300ms, *p*=.0499; 12Hz, -700ms to 0ms, *p*=.0020) and continued into the beta band (13Hz, -700ms to 0ms, *p*=.0080; 14Hz, -650ms to -50ms, *p*=.0300). Additional post-hoc analyses were aimed at further investigating the interaction between confidence and stimulus presence. There was an increase in beta power preceding high confidence false percepts (-650ms to 0ms, *p*=.0108, cluster-based permutation-test) (Fig. 2a). This effect was not significant for pre-stimulus alpha (-650ms to -150ms, *p*=.11). Follow-up analyses estimating the effects for each frequency in steps of 1Hz revealed that the effect ranged from 11-14 Hz (11Hz, -700ms to 0ms, *p*=.0039; 12Hz, -700ms to 0ms, *p*=.0059; 13Hz, -750ms to -150ms, *p*=.0079; 14Hz, -

700ms to -400ms, *p*=.049). Thus, the increase in power preceding high confidence false percepts was in the high alpha, low beta band (Fig. 2b). In contrast, no effects were found comparing high and low confidence reports on grating-present trials for either alpha and beta power, *p*>.5, Fig. 2d). No effects were found in the post-stimulus time-window for either false or veridical percepts (*p*>.5). Thus, in sum, an increase in high alpha/low beta band power preceded high confidence false percepts, but not high confidence veridical percepts.
We performed source localisation analyses on the difference in beta power prior to high and low confidence false percepts in the -750 to 0ms pre-stimulus time window centred around 13Hz (+- 1.5 Hz). This revealed that the increase in beta power arose from a network including parietal and occipital regions (Fig. 2c).

A shared neural code reflecting confidence in stimulus presence emerged 250ms post-stimulus
We next decoded confidence in stimulus presence on both grating-present and noise-only trials using an LDA (Mostert et al., 2015). Across both grating-present and noise-only trials, a confidence signal emerged 265ms post stimulus and was sustained throughout the post-stimulus window (265ms-2000ms, *p*<.001, Cohen's d= 1.6) (Fig. 3a). This signal was present on both noise-only (410ms-1280, 1280-2000ms, *p*<.001, Cohen's d= 1.1, 1.2) (Fig. 3b) and grating-present trials (425ms-670, 700-2000ms, *p*<.001, Cohen's d= 0.83, 1.26) (Fig. 3c). To test whether the neural representation of perceptual confidence in veridical and false percepts was the same, we trained on perceptual confidence on noise-only trials, and decoded the confidence on grating-present trials, and vice versa. Cluster-based analyses on the diagonal revealed a significant effect in the post-stimulus time window, demonstrating that the confidence signal on noise-only trials generalised to grating-present trials (235ms-385ms, 415ms-470ms, 480ms-2000ms, *p*<.001, Cohen's d= 0.85, 0.76, 1.38) (Fig. 3d) and vice versa (225ms-295ms, 320ms-385ms, 415ms-875ms, 885ms-1000ms, *p*=.008, .015, .001, .003, Cohen's d= 0.93, 0.81, 1.26, 1.19) (Fig. 3e).
To ensure that the decoding results were not confounded by unequal numbers of low and high confidence trials, we repeated the analyses drawing a random number of trials from the overrepresented condition equal to the number of trials in the underrepresented condition. In some individuals this led to very few trials to perform the decoding analyses on, leading to unreliable results. We therefore removed participants with fewer than 50 trials to train the decoder on. We found significant decoding of confidence post-stimulus in all conditions (all trials: 260ms (Fig. 3f).
For visualisation purposes, we reconstructed the source of the confidence signal by performing source localisation separately on the magnetic fields underlying high and low confidence perceptual reports and computing a signal difference map. This was then overlayed on a 3D cortical surface. This source reconstruction was conducted on the 1000-2000ms time window, where decoding was the strongest. These analyses revealed that on a group-level the source contributing to perceptual confidence were arising from parietal and frontal regions for both noise-only and grating-present trials (Fig. 3g).

ERF analyses
Finally, we performed ERF analyses to explore whether confidence in stimulus presence was reflected in the raw ERF signal on grating-present and noise-only trials. For these purposes we contrasted high and low confidence trials, and computed cluster-based analyses on these differences. There was no effect of confidence on the raw ERF signal on the sensor level on either noise-only or grating-present trials (*p*>.5).

Discussion

The present study explored the divergence and convergence of the neural dynamics underlying veridical and false perception. During a perceptual discrimination task, participants indicated whether they perceived a grating with a specific orientation. On a subset of noise-only trials, participants reported seeing gratings with high confidence, which we dubbed high confidence false percepts. We found that high confidence false percept trials were preceded by increased alpha/low beta-power relative to low confidence percepts, arising from a parietal occipital network. This effect was not present for high confidence veridical percepts, suggesting a unique mechanism contributing to false percepts. Post stimulus, LDA analyses revealed a perceptual confidence signal emerging ~250ms post-stimulus on both veridical and false percept trials. This neural signal was shared between veridical and false perception, as revealed by cross-decoding analyses between false and veridical percepts, suggesting an early final common pathway between veridical and false perception following initial diverging temporal dynamics. Source localisation of this signal revealed that it arose mostly from parietal and frontal regions.

What could the role of increased alpha/beta power be in driving high confidence false percepts? As discussed above, in stimulus detection paradigms, it is well known that a decrease in alpha and beta power is related to increased hit rates (Achim et al., 2013; Benwell et al., 2017; Boncompte et al., 2016; Brüers & VanRullen, 2018; Chaumon & Busch, 2014; Ergenoglu et al., 2004; Mathewson et al., 2014; Samaha et al., 2017, 2020; Van Dijk et al., 2008). However, some studies have found the opposite for false percepts, where it is an increase in beta power, rather than a decrease, that drives false percepts (Keil et al., 2014; Poorganji et al., 2023). This suggests that the mechanism underlying perceptual thresholds for external stimuli (increased excitability) might be different from those for internally driven false percepts. One possible mechanism is suggested by previous studies which have linked high alpha/beta power to top-down endogenous signals. A number of studies have substantiated this, linking high alpha/beta power – often arising from the parietal cortex – to attention, imagination, illusory perception, and prediction (Arnal & Giraud, 2012; Auksztulewicz et al., 2017; Bartsch et al., 2015; Bastos et al., 2020; Buschman & Miller, 2007, 2009; De Lange et al., 2013; Engel & Fries, 2010; Fujioka et al., 2012; Hipp et al., 2011; Iversen et al., 2009; Okazaki et al., 2008; Pesaran et al., 2008; Raposo et al., 2023; Sherman et al., 2016; Villena-González et al., 2018). Moreover, previous fMRI studies have reported lower BOLD activity prior to false percepts (Hesselmann et al., 2010; Pajani et al., 2015). Because alpha/beta power and BOLD activity are inversely correlated (Scheeringa et al., 2011, 2016), speculatively, increased alpha/beta power might have played a role in these fMRI studies as well. However, this does not answer the question of what mechanism underlies fluctuations in beta power in the present study. Speculatively, they might reflect beliefs about stimulus presence. That is, while the specifically cued orientations (e.g., a low tone predicts a left-tilted grating) did not influence which orientation participants reported on high confidence false percepts trials, there was likely still a strong expectation of *a grating* (of either orientation) being present on each trial, as the participants were not explicitly told that there would be noise-only trials. This was confirmed by participants grossly underestimating the proportion of noise-only trials upon debriefing. As previous studies have linked an increase in beta power to stimulus predictions (Auksztulewicz et al., 2017; Bastos et al., 2020; Fujioka et al., 2012;

Turner et al., 2023), we speculate here that beta power may reflect endogenous trial-by-trial fluctuations in stimulus expectation, which may have contributed to the high confidence false percepts in this study. Additionally, top-down mechanisms like imagination or choice history could have added to these effects (Dijkstra & Fleming, 2023; Urai et al., 2019). Future research could target this question by manipulating these mechanisms explicitly.

A previous study of ours used the same paradigm to study false percepts, but using layer-specific fMRI rather than MEG (Haarsma et al., 2022). Notably, the behavioural findings across these two studies were highly consistent, with both reporting a limited effect of cued orientations on perception, which was only significant in those who became aware of the meaning of the auditory cues. Regardless, in both studies participants reported high confidence false percepts on noise-only trials in almost identical proportions (35% and 36% in the present and previous study, respectively). In the layer-specific imaging study, we found that the content of false percepts was reflected in the middle layers of the early visual cortex, suggesting a feedforward signal driving the content of false percepts. Together with the findings of the present study, we speculate that on noise-only trials, enhanced alpha/beta power and stimulus-specific activity fluctuations in the early cortex work in concert to generate high confidence false percepts, potentially by enhancing these signals in the middle layers. In line with this, alpha/beta power partly source localised to the occipital cortex, making it ideally situated to interact with orientation-specific signals in the early visual cortex. Indeed, previous studies have linked interaction between these areas to the modulation of sensory activity by priors (Rahnev et al., 2011). The nature of this potential interaction between alpha/beta oscillations and stimulus-specific activity fluctuations requires much further investigation.

A final common pathway reflecting perceptual confidence emerged post-stimulus. This became significant around 250ms post-stimulus and remained significant throughout the post-stimulus time-window. One might argue that this signal reflects motor preparation, potentially due to a facilitated motor response on high confidence trials. However, this is unlikely, due to the randomised stimulus-response mapping employed in the current study, which precluded the possibility of preparing a motor response. Instead, the uncovered neural signal is likely to track confidence in the presence of a stimulus. Previous studies using variations of perceptual discrimination and detection tasks have reported neural correlates of perceptual confidence signals originating from the dorsolateral and (ventral) medial prefrontal cortex (Bang et al., 2020; Bang & Fleming, 2018; Gherman & Philiastides, 2018; Lau & Passingham, 2006; Shekhar & Rahnev, 2018; Yeon et al., 2020). Note that confidence here reflected the degree to which one was certain a stimulus was present, and is therefore strongly linked to stimulus visibility, which previous studies have shown to be encoded in frontal regions (Mazor et al., 2022). A likely neuromodulatory system that contributes to this signal is the dopamine system, which extensively innervates frontal regions (Björklund & Dunnett, 2007). Indeed, a series of studies have shown that dopamine may play an important role in modulating perceptual confidence, with dopaminergic agonists increasing confidence in perceptual detection (Lou et al., 2011). In rats, causally manipulating dopamine modulates confidence in false alarms (Schmack et al., 2021). Further, in primates, subjective stimulus intensity is reflected by the dopamine signal (De Lafuente & Romo, 2011). Most relevantly, a dopaminergic perceptual confidence signal in the caudate emerges around 300ms post-stimulus during decision-making (Lak et al., 2017), aligning with the emergence of the

confidence signal in our cluster-based analyses. However, it should be noted that cluster-based analyses preclude exact inferences about the latency of signals (Maris & Oostenveld, 2007; Sassenhagen & Draschkow, 2019).

In conclusion, the present study revealed increased high alpha/low beta power arising from a parietal occipital network specifically preceding high confidence false percepts, but not veridical perception. Subsequently, a final common pathway reflecting perceptual confidence shared by veridical and false percepts emerged around 250ms post-stimulus in the parietal and frontal cortices. Thereby, the current study sheds light on how false and veridical percepts initially have diverging mechanisms but subsequently converge in higher-order regions to lead to seemingly qualitatively similar experiences.

Figures

Fig. 1 | Experimental design and behavioural findings. a, An auditory cue was followed by either a low contrast grating embedded in noise (50% of trials), or a noise patch (50%). Participants indicated which orientation they saw and how confident they were that a grating was presented. **b**, One sound predicted the appearance of a 45°, or clockwise, oriented grating, whilst the other predicted a 135°, or anti-clockwise, orientated grating. Auditory cues were 100% valid on grating-present trials. **c,** Participants were more accurate on high confidence trials. **d,** Upon debriefing participants believed that only 18% of trials contained noise, compared to the real number of 50%. **e,** Participants were driven by the cue on noise-only trials when they were aware of the cues meaning. **f,** On noise-only trials, participants believed there to be a grating on 35% of trials.

Fig. 2 | Frequency analyses. a, Scalp topographies of differences in pre-stimulus beta power for high minus low confidence false percepts . **b,** Difference in average time x frequency between high and low confidence trials on noise-only trials. **c,** T-map of the difference in source localisation for the 13Hz frequency band +- 1.5Hz between high and low confidence response on noise-only trials. A network of parietal and occipital regions was active prior to high confidence false percepts. **d,** Difference in average time x frequency between high and low confidence trials on grating-present trials.

Fig. 3 | Decoding of perceptual confidence. A linear discriminator analyses was used to identify a perceptual confidence signal. **a,** A significant confidence signal was found on all trials after stimulus onset. Analysing noise-only **(b)** and grating-present **(c)** trials separately revealed similar results. Cross-decoding from noise-only to grating-present trials **(d),** and vice versa **(e),** demonstrated that there was a shared neural signal on grating-present and noise-only trials. **f,** When balancing low and high confidence trial counts decoding was still successful, demonstrating that the effect was not confounded by imbalanced trial counts. **g,** Percentage absolute signal change of the high confidence condition compared to the low confidence condition in source localisation. Here the combined, noise-only, and grating-present trials in the 1000ms to 2000ms time window are presented separately. Across all three conditions, parietal and frontal cortices contributed most strongly to the linear discrimination analyses. S = onset of stimulus, Or = onset orientation response cue, Cr = onset of confidence response cue.

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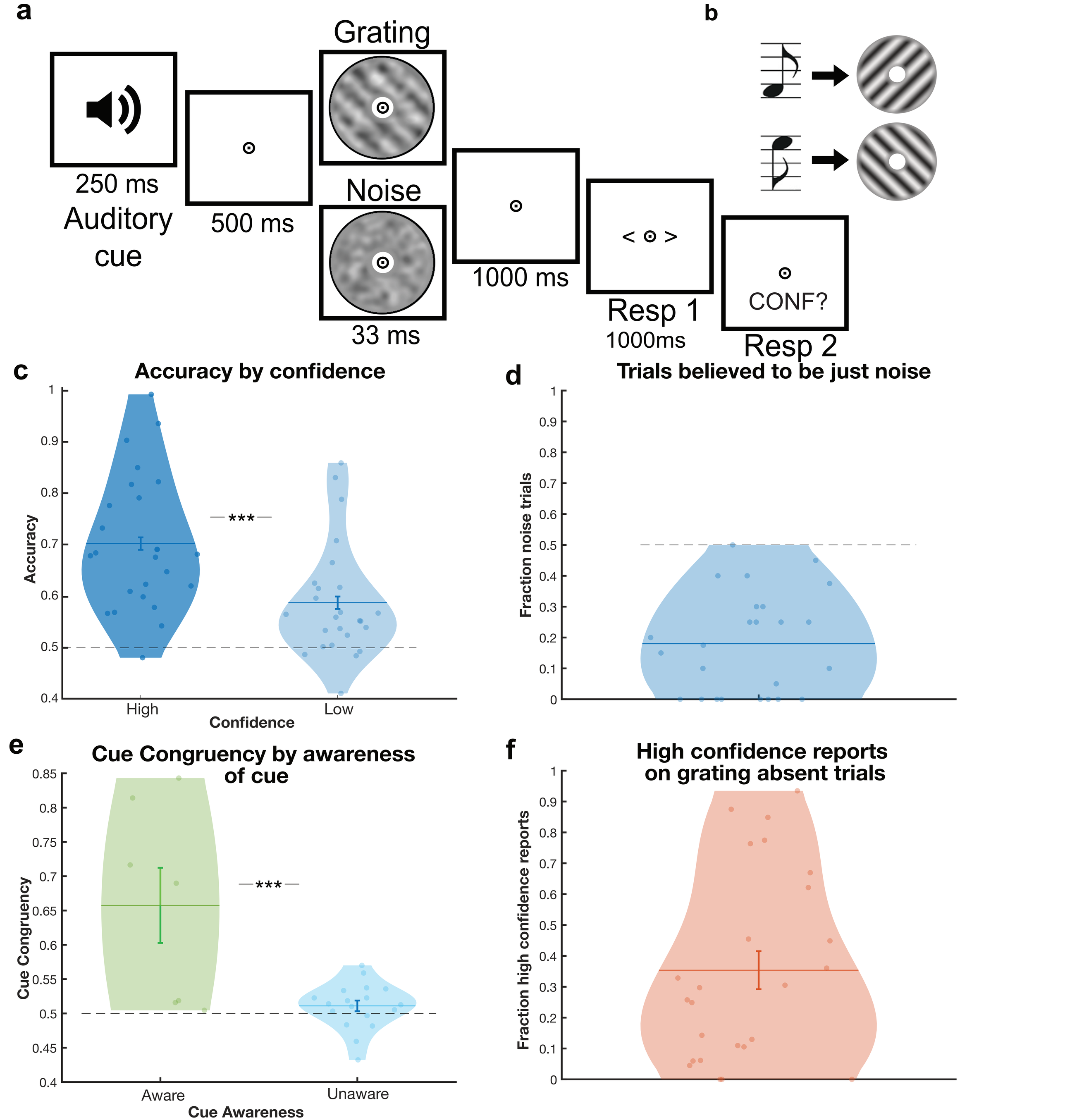
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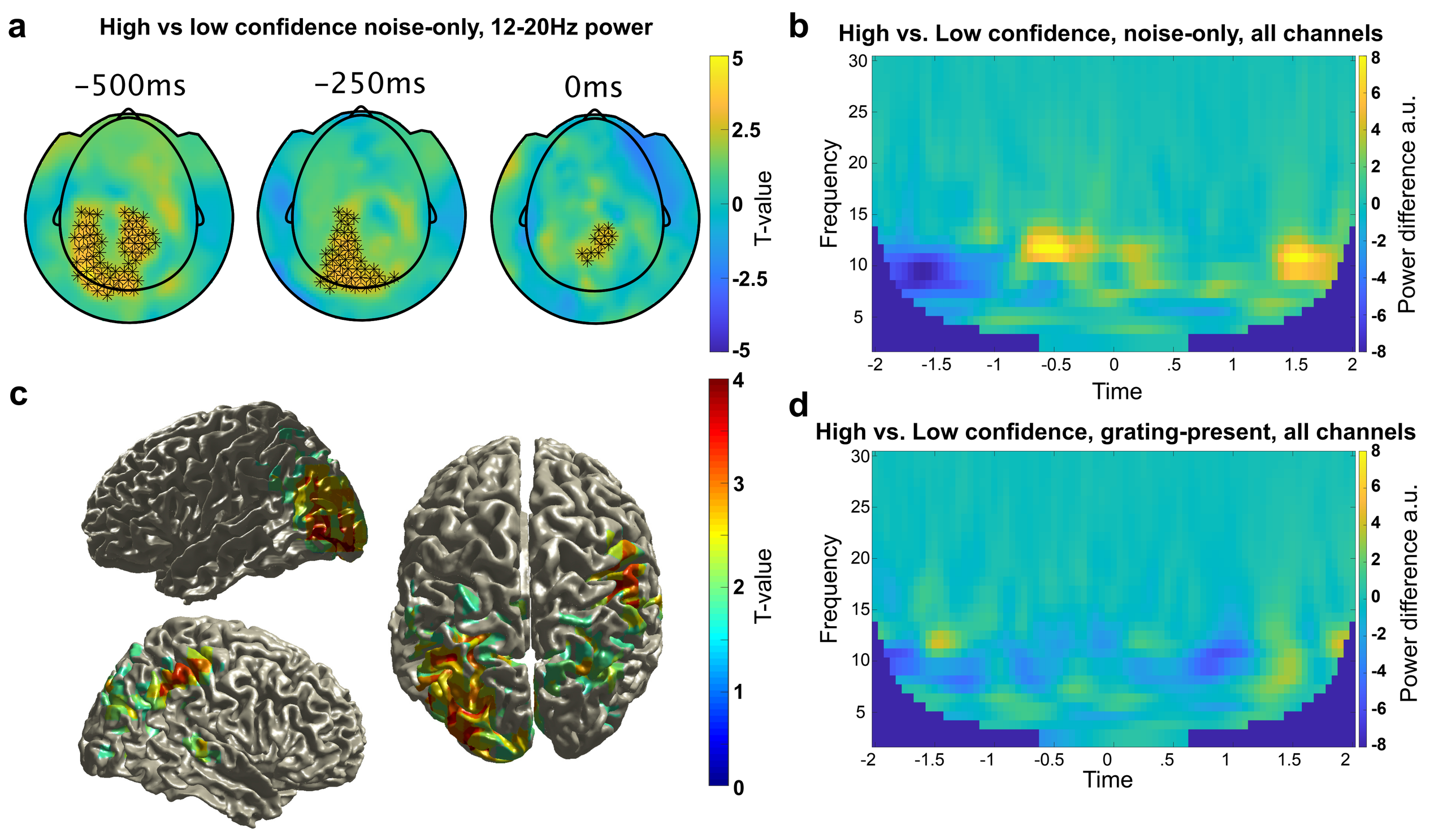
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-2.5
-5
T-value
b
High vs. Low confidence, noise-only, all channels
Frequency
Time
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High vs. Low confidence, grating-present, all channels
Frequency
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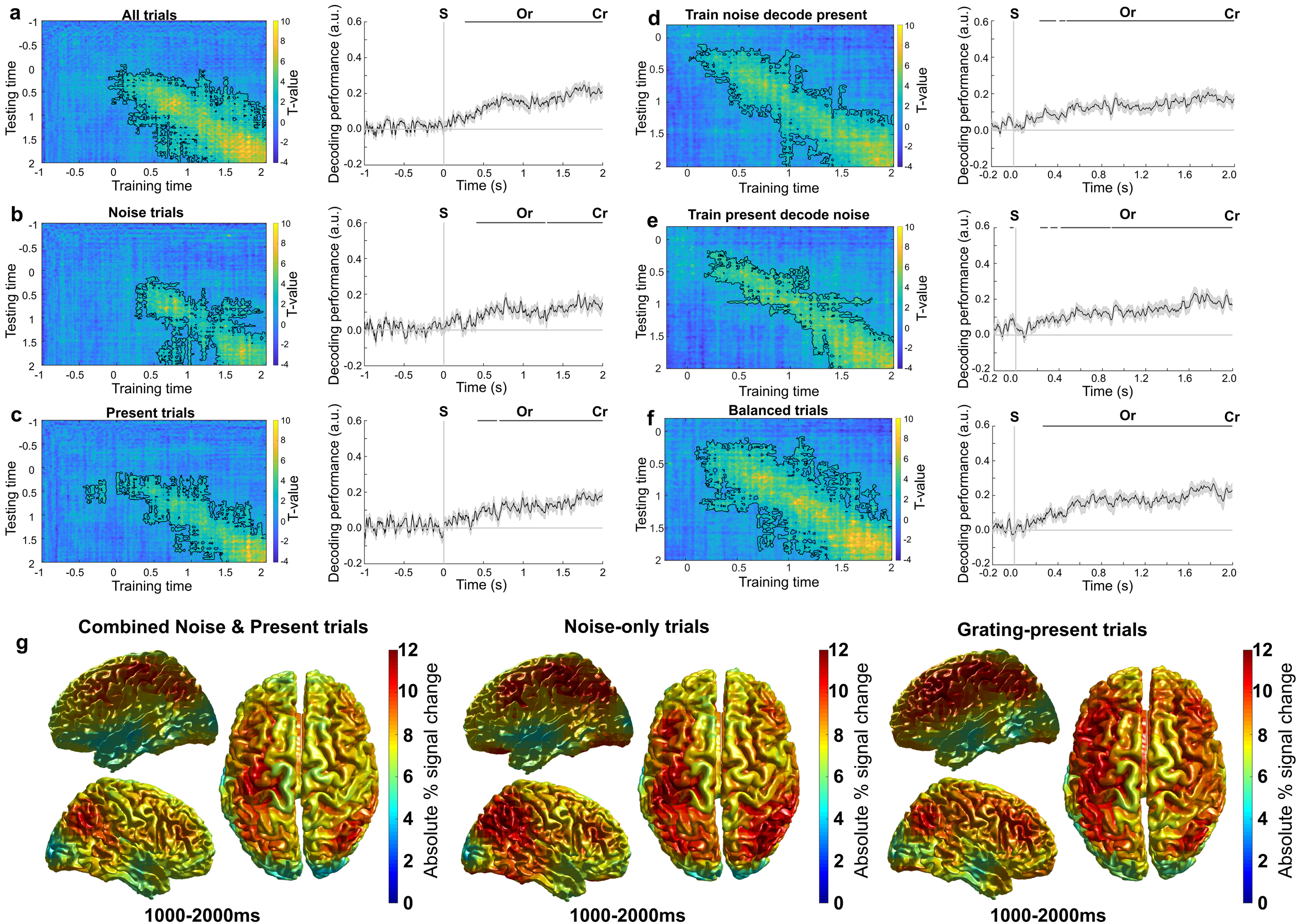
a
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b
Noise trials
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Noise-only trials
Grating-present trials
Testing time
Training time
T-value
Decoding performance (a.u.)
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