1 **Thalamic Network Controllability Predicts Cognitive Impairment**
2 **in Multiple Sclerosis**

Running title: Thalamic network controllability predicts CIMS

Yuping Yang[1], Anna Woollams[1], Ilona Lipp[2], Zhizheng Zhuo[3], Marta Czime Litwińczuk[1],

Valentina Tomassini[4], Yaou Liu[3*], Nelson J Trujillo-Barreto[1,5*], Nils Muhlert[1*]

[1]Division of Psychology, Communication and Human Neurosciences, Faculty of Biology,

Medicine and Health, University of Manchester, Manchester, UK

[2]Department of Neurophysics, Max Planck Institute for Human Cognitive and Brain Sciences,

Leipzig, Germany

[3]Department of Radiology, Beijing Tiantan Hospital, Beijing, China

[4]Institute for Advanced Biomedical Technologies (ITAB), Department of Neurosciences,

Imaging and Clinical Sciences, University G. d'Annunzio of Chieti-Pescara, Chieti, Italy

[5]School of Psychology, Faculty of Health and Education, Manchester Metropolitan

University, UK

[*]These authors contributed equally to this work as joint senior authors

Correspondence to:

Dr Nils Muhlert, Division of Psychology, Communication and Human Neurosciences,

Faculty of Biology, Medicine and Health, University of Manchester, Oxford Road,

Manchester M13 9PL, UK, E-mail: nils.muhlert@manchester.ac.uk

Yuping Yang, Division of Psychology, Communication and Human Neurosciences, Faculty

of Biology, Medicine and Health, University of Manchester, Oxford Road, Manchester M13

9PL, UK, E-mail: yuping.yang@manchester.ac.uk

Abstract:

Recent research suggests that individuals with multiple sclerosis (MS) and cognitive impairment exhibit more effortful and less efficient transitions in brain network activity. Previous studies further highlight the increased vulnerability of specific regions, particularly the thalamus, to disease-related damage. This study investigates whether MS affects the controllability of specific brain regions in driving network activity transitions across the brain and examines the relationship between these changes and cognitive impairment in patients. Resting-state functional MRI and neuropsychological data were collected from 102 MS and 27 healthy controls. Functional network controllability analysis was performed to quantify how specific regions influence transitions between brain activity patterns or states. Disease alterations in controllability were assessed in the main dataset and then replicated in an independent dataset of 95 MS and 45 healthy controls. Controllability metrics were then used to distinguish MS from healthy controls and predict cognitive status. MS-specific controllability changes were observed in the subcortical network, particularly the thalamus, which were further confirmed in the replication dataset. Cognitively impaired patients showed significantly greater difficulty in the thalamus steering brain transitions towards difficult-to-reach states, which are typically associated with high-energy-cost cognitive functions. Thalamic network controllability proved more effective than thalamic volume in distinguishing MS from healthy controls (AUC = 88.3%), and in predicting cognitive status in MS (AUC = 80.7%). This study builds on previous research highlighting early thalamic damage in MS, aiming to demonstrate how this damage disrupts activity transitions across the cerebrum and may predict cognitive deficits. Our findings suggest that the thalamus in MS becomes less capable of facilitating broader brain activity transitions essential for high-energy-cost cognitive functions, implying a potential pathological mechanism that links thalamic functional changes to cognitive impairment in MS.

Keywords: multiple sclerosis; cognitive impairment; thalamus; subcortical network; network controllability; resting-state fMRI

Abbreviations:

AUC = Area under curve; BRB-N = Brief Repeatable Battery of Neuropsychological Tests; CIMS = cognitively impaired multiple sclerosis; CPMS = cognitively preserved multiple sclerosis; DAN = dorsal attention network; DMN = default mode network; EDSS = Expanded Disability Status Scale; FA = flip angle; FLAIR = fluid-attenuated inversion recovery; FPN = frontoparietal network; HC = healthy control; LN = limbic network; MS = multiple sclerosis; MSFC = Multiple Sclerosis Functional Composite; PASAT3 = Paced Auditory Serial Addition Task 3 seconds; ROC = receiver operating characteristic; rs-fMRI = resting-state functional MRI; SD = standard deviation; SMN = somatomotor network; VAN = ventral attention network; VN = visual network; 25-FWT = 25 Foot Walk Test; 3DT1 = 3D T1-weighted sequence; 9-HPT = 9 Hole Peg Test.

Introduction

Cognitive impairment is common in multiple sclerosis (MS), with estimated prevalence ranging from 43% to 70%.[1] Previous studies suggest that cognitive impairments in MS arise due to brain changes in specific neural networks.[2–10] A useful recent model indicates that MS patients with cognitive impairment (CIMS), in comparison to cognitively preserved patients (CPMS), exhibit less frequent transitions between brain states (regional activity patterns) and show subcortical-related functional connectivity changes.[5] Subcortical network has gained wide attention in MS, with many studies reporting associations between cognitive impairment and network changes in subcortical regions, such as the thalamus.[6–8,10] Central to these findings is the idea that subcortical regions, particularly the thalamus, are affected early in the course of MS;[11–15] as the disease progresses, neurodegeneration and functional network changes seem to spread from the thalamus towards the broader brain.[16] This early involvement of the thalamus may drive the subsequent changes in the other parts of the brain, leading to a widespread disruption of brain activity and causing reduced efficiency in brain function.

An emerging approach that allows characterizing how specific brain regions influence network activity in the rest of the brain is 'network controllability' analysis.[17–19] This approach allows moving beyond assessing changes in regional activity, towards identifying the brain regions driving those changes and how they influence the transitions between brain states (regional activity patterns of the brain). Network controllability has been validated as a powerful tool in exploring clinical biomarkers in neurological and neuropsychological diseases.[20–24] In MS, a recent study showed that it became more effortful for cognitively impaired patients to transition between brain states.[25] However, current knowledge has not yet addressed whether and how MS alters the controllability of specific brain regions in facilitating transitions across the brain, and how these alterations predict cognitive impairment in patients.

To fill this gap, this study applied widely used controllability measures to two independent MS datasets to examine how different regions impact brain state transitions. These measures were further evaluated as predictors of cognitive impairment in MS and for their potential to support clinical diagnosis. We hypothesize that: (i) MS patients exhibit regions less effective in facilitating brain state transitions, as reflected in disease-related controllability changes; (ii) these changes are concentrated in those brain regions associated

93 with cognitive dysfunction in MS, such as the thalamus; (iii) are more pronounced in

94 cognitively impaired patients; and (iv) can help predict cognitive impairment and aid clinical

95 diagnosis.

Materials and Methods

Participants

Main dataset

The main dataset involved 102 patients with relapsing-remitting MS recruited from the Helen

Durham Centre for Neuroinflammation at the University Hospital of Wales and 27 healthy

controls (HC) recruited from the local community. All participants were aged between 18 and

60 years, right-handed, and devoid of contraindications for MR scanning. Additional

eligibility criteria were required for the patients including the absence of comorbid

neurological or psychiatric disease, no modifications to their treatments within three months

prior to the MRI scanning, and being in a relapse-free phase. All participants underwent

demographic information collection, clinical and psychological assessments, and MRI

scanning in one study session. This study was approved by the NHS South-West Ethics and

the Cardiff and Vale University Health Board R&D committees. Written informed consent

was obtained from each participant.

Replication dataset

The replication dataset included 95 patients with relapsing-remitting MS recruited from the

Beijing Tiantan Hospital and 45 HC recruited from the local community. The participants

were aged between 17 and 80 years, right-handed, and devoid of contraindications for MR

scanning. Additional exclusion criteria were employed including incomplete MRI images,

poor image quality, and a history of comorbid neurological or psychiatric disease. All

participants underwent demographic information collection, clinical assessments, and MRI

scanning in one study session. This study was approved by the Institutional Review Board of

the Beijing Tiantan Hospital, Capital Medical University, Beijing, China. Written informed

consent was obtained from each participant.

Demographic, Clinical and Neuropsychological Assessment

Demographic and clinical data for both datasets included age, sex, education level, disease

duration and the Expanded Disability Status Scale (EDSS) scores. The main dataset had

additional clinical scores assessed using the Multiple Sclerosis Functional Composite (MSFC)

as well as neuropsychological scores of four cognitive domains assessed using the Brief

Repeatable Battery of Neuropsychological Tests (BRB-N) as described previously.[4] Patients

from the main dataset were classified into CIMS and CPMS according to previous studies.[4,26]

Specifically, CIMS patients were defined as those who scored $\geq$ 1.5 SDs below the control

mean on at least 2 subtests of BRB-N, while the others were defined as CPMS. The scores of

each of the four cognitive domains were calculated by averaging the scores of all subtests

assigned in that domain. The global cognitive function score (global BRB-N) was calculated

by averaging the scores of all four cognitive domains.

MRI Acquisition

Main dataset

MRI data were acquired on a 3T MR scanner (General Electric HDx MRI System, GE

Medical Devices, Milwaukee, WI) with an 8-channel receive-only head radiofrequency coil.

A high-resolution 3D T1-weighted sequence (3DT1) was acquired for identification of T1-

hypointense MS lesions, segmentation, and registration (voxel size = 1 mm $\times$ 1 mm $\times$ 1 mm,

echo time [TE] = 3.0 ms, repetition time [TR] = 7.8 ms, matrix size= 256 $\times$ 256 $\times$ 172, field

of view [FOV] = 256 mm $\times$ 256 mm, flip angle (FA) = 20°). A T2/proton density–weighted

sequence (voxel size = 0.94 mm $\times$ 0.94 mm $\times$ 4.5 mm, TE = 9.0/80.6 ms, TR = 3,000 ms,

FOV = 240 mm $\times$ 240 mm, number of slices = 36, FA = 90°) and a fluid-attenuated inversion

recovery (FLAIR) sequence (voxel size = 0.86 mm $\times$ 0.86 mm $\times$ 4.5 mm, TE = 122.3 ms, TR

= 9,502 ms, FOV = 220 mm $\times$ 220 mm, number of slices = 36, FA = 90°) were acquired for

identification and segmentation of T2-hyperintense MS lesions. Resting-state functional MRI

(rs-fMRI) was acquired with a T2*-weighted gradient-echo echo-planar imaging sequence

(voxel size = 3.4 mm $\times$ 3.4 mm $\times$ 3 mm, TE = 35 ms, TR = 3,000 ms, matrix size = 64 $\times$ 64 $\times$

46, FOV = 220 mm $\times$ 220 mm, number of volumes = 100, number of slices = 46, interleaved

order). All participants were instructed to relax with their eyes closed during rs-fMRI

scanning.

Replication dataset

MRI data were acquired on a 3T MR scanner (Philips CX, Best, The Netherlands) including

3DT1, FLAIR, and rs-fMRI. 3DT1 image was acquired using sagittal acquisition with

magnetization-prepared rapidly acquired gradient echo (voxel size = 1 mm × 1 mm × 1 mm,

echo time [TE] = 3.0 ms, repetition time [TR] = 6.6 ms, matrix size = 196 × 256 × 170,

inversion recovering = 880 ms, FA = 8°). FLAIR sequence was acquired using 3D sagittal

acquisition with inversion recovering fast spin echo (voxel size = 1 mm × 1 mm × 1 mm, TE

= 228 ms, TR = 4,800 ms, inversion time = 1650 ms, FA = 90°). rs-fMRI image was acquired

using 2D axial acquisition with field echo EPI (voxel size = 3 mm × 3 mm × 3 mm, TE = 30

ms, TR = 2,000 ms, matrix size= 80 × 80 × 40, number of volumes = 180, number of slices =

40, interleaved order, slice thickness = 3 mm, slice gap = 0.3 mm, FA = 78°) during which all

participants were instructed to relax with their eyes closed.

MRI preprocessing

Lesion filling was performed on the structural 3DT1 images of patients as previously

described,[4] followed by segmentation into grey matter, white matter, and cerebrospinal fluid

using SPM12 (v7771) toolbox (http://www.fil.ion.ucl.ac.uk/spm/software/spm12/). The

quality of segmentation was assessed manually. rs-fMRI preprocessing was also performed

using SPM12. Briefly, individual functional images were first corrected for head motion and

acquisition time offsets between slices. No significant differences were found in the

maximum and mean frame-wise displacement of head motion between groups in both the

main and replication datasets ($p > 0.05$, permutation test). The corrected images were then

spatially normalized to the MNI space by applying deformation fields derived from tissue

segmentation of structural images. All normalized images further underwent spatial

smoothing by a Gaussian kernel with 6-mm full width at half maximum.

Functional network controllability analysis

We included 400 cortical[27] and 54 subcortical regions[28] to calculate functional connectivity

networks based on pair-wise Pearson correlation between the time series of all regions. Then,

network controllability measures, including average controllability, modal controllability and

activation energy, were calculated to quantify how a specific region can influence brain-wide

dynamics (Figure 1; See Supplementary Methods for details).[18,19] Specifically, average

controllability measures how easily a brain region move the brain into nearby or easily

reachable states, which reflects the brain capacity for low-energy-cost and frequent small

adjustments in brain states.[17–19] Modal controllability, on the contrary, measures a region's

ability to move the brain into difficult or unstable states, which is important for executing

high-energy-cost large transitions in brain activity (e.g. between resting and active states).[17–

19] Regional activation energy captures the feasibility or minimum energy required by the

given region to induce a transition between brain states.[17–19] To facilitate interpretation and

comparison, region-level controllability measures were averaged into global (whole brain),

cortical and subcortical network levels. Cortical network controllability measures were

averaged into seven resting-state functional networks,[29] including the visual network (VN),

somatomotor network (SMN), dorsal attention network (DAN), ventral attention network

(VAN), limbic network (LN), frontoparietal network (FPN) and default mode network

(DMN). Similarly, subcortical network controllability measures were averaged into seven

anatomical nuclei, namely the hippocampus, thalamus, amygdala, caudate, nucleus

accumbens, putamen and globus pallidus.[28]

Statistical analysis

Statistical analyses were performed using MATLAB software version R2022b (MathWorks,

Inc). A 95% confidence interval was used for each effect. Chi-squared tests were used to

compare dichotomous variables (sex). The group comparisons of continuous demographic,

clinical, neuropsychological and network controllability variables were performed by

permutation tests (10,000 permutations). Age and sex were considered as covariates for

neuropsychological and network controllability variables. FDR corrections were performed

for multiple comparisons. See Supplementary Methods for details.

Classification analysis

We trained linear SVM classifiers to distinguish between MS and controls, as well as between

MS with different cognitive status (CIMS vs. CPMS) and between MS with different level of

disability (EDSS < 4.0 vs. EDSS ≥ 4.0). Controllability and/or volumetric measures were

used as predictive features. A set of performance metrics, including accuracy, precision,

sensitivity, specificity, and area under the curve (AUC) were computed to access the

performance of the classifiers. See Supplementary Methods for details.

Results

Demographic, clinical, and neuropsychological characteristics

Main dataset

The MS group was significantly older, had lower education levels, and exhibited worse performance on all subtests of the MSFC as well as all four cognitive domains of the BRB-N than HC group ($p < 0.05$, FDR corrected). Across all patients, 55 were identified as CIMS and 47 as CPMS. CIMS showed worse performance on 9-HPT, PASAT3 and all four cognitive domains than CPMS and HC ($p < 0.05$, FDR corrected). No differences were found between CPMS and HC on cognitive performance (Table 1).

Replication dataset

The MS group was significantly younger and had lower education level than HC group ($p < 0.05$, FDR corrected; Supplementary Table S1). Due to the differences in the cognitive assessment scales between the main and replication datasets, further subgroup splitting in terms of CIMS and CPMS were not available on the replication dataset.

Network controllability changes in MS

Main dataset

Significant controllability changes in MS were predominately localized in the subcortical network, particularly in the thalamus. Specifically, at the global (whole brain) level, MS group showed increased average controllability ($p < 0.001$), decreased modal controllability ($p = 0.008$) and decreased activation energy ($p = 0.016$) compared to HC group. When looking at the eight resting-state networks, controllability changes were primarily localized within the subcortical network. Specifically, MS group exhibited increased average controllability ($p = 0.001$), decreased modal controllability ($p = 0.002$) and decreased activation energy ($p < 0.001$) in the subcortical network, compared to HC group (Figure 2). When looked at each of the seven nuclei within the subcortical network separately, the subcortical changes were predominately due to the changes within the thalamus. Specifically, MS group showed increased average controllability ($p < 0.001$), decreased modal controllability ($p = 0.005$) and decreased activation energy ($p = 0.007$) in the thalamus compared to HC (Figure 3). Decreased activation energy was also found in the globus pallidus in MS ($p = 0.004$; Supplementary Figure S1). For the cortical networks, MS-related controllability changes were only found regarding average controllability (VN, SMN, DAN, VAN, FPN and DMN: $p < 0.05$), no differences were observed in any cortical networks

242   regarding modal controllability or activation energy (Supplementary Figure S2).

Replication dataset

Consistent with the main dataset, significant controllability changes in MS were primarily
localized in the subcortical network and thalamus in the replication dataset. Specifically, MS
exhibited replicated increases in average controllability ($p = 0.005$) in the subcortical network
compared to HC (Figure 2). When looked at each of the seven nuclei within the subcortical
network separately, MS group showed replicated increases in average controllability ($p =$
0.027) in the thalamus compared to HC (Figure 3). Additionally, increases in average
controllability were also observed in other subcortical nuclei, including caudate, nucleus
accumbens and putamen ($p < 0.05$, Supplementary Figure S3). No MS-related controllability
changes were found in any of the cortical networks.

Network controllability changes in CIMS and CPMS

Significant controllability differences between CIMS and CPMS were only observed in the
thalamus. Specifically, at the whole brain level, both CIMS and CPMS showed increased
average controllability (CIMS: $p = 0.002$; CPMS: $p < 0.001$), while CIMS additionally
exhibited decreased modal controllability ($p = 0.009$) and decreased activation energy ($p =$
0.016) compared to HC. When looked at the eight networks, both CIMS and CPMS showed
increased average controllability (CIMS: $p < 0.001$; CPMS: $p = 0.008$), decreased modal
controllability (CIMS: $p = 0.006$; CPMS: $p = 0.008$) and decreased activation energy (CIMS:
$p = 0.007$; CPMS: $p = 0.003$) in the subcortical network compared to HC (Figure 4). When
further looked at the seven nuclei within the subcortical network, while both CIMS and
CPMS showed increased average controllability in the thalamus (CIMS: $p < 0.001$; CPMS: p
$= 0.009$), CIMS exhibited significantly higher increases in thalamus than CPMS ($p = 0.016$,
Figure 5). Additionally, only the CIMS group, but not CPMS, showed significant decreases in
modal controllability ($p = 0.002$) and activation energy ($p = 0.006$) in the thalamus compared
to HC (Figure 5). No significant differences were observed between CIMS and CPMS when
examining any other parts of the brain aside from the thalamus.

Classification performance

Thalamic network controllability measures demonstrated superior classification performance
compared to thalamic volume in distinguishing between MS and controls, as well as between

MS with different cognitive status and between MS with different level of disability (Figure 6,

Table 2). Specifically, classifiers based on both thalamic network controllability and thalamic

volume achieved an AUC of 88.3% in distinguishing MS from HC (precision = 93.9%;

accuracy = 80.9%; sensitivity = 81.1%; specificity = 80.2%), outperforming those based on

thalamic volume alone, which achieved an AUC of 74.5% (precision = 88.8%; accuracy =

68.1%; sensitivity = 68.3%; specificity = 67.6%). Moreover, in differentiating CIMS and

CPMS, classifiers based on the thalamic network controllability measures alone achieved an

AUC of 80.7% (precision = 75.4%; accuracy = 72.4%; sensitivity = 72.7%; specificity =

72.0%), outperforming those based on the combination of both controllability and volume

classifiers (AUC = 68.2%; precision = 64.6%; accuracy = 61.7%; sensitivity = 64.5%;

specificity = 58.4%), whereas volumetric classifiers alone failed to differentiate CIMS and

CPMS (AUC = 38.2%; precision = 45.3%; accuracy = 41.6%; sensitivity = 41.2%; specificity

= 42.1%). Besides, in differentiating MS with different level of disability, classifiers based on

the thalamic network controllability measures achieved an AUC of 82.9% (precision = 77.2%;

accuracy = 76.3%; sensitivity = 82.4%; specificity = 68.2%), outperforming those based on

thalamic volume, which achieved an AUC of 67.8% (precision = 69.3%; accuracy = 64.7%;

sensitivity = 67.4%; specificity = 61.2%).

Discussion

Our study demonstrated altered functional network control from the thalamus in people with

MS, which can be used to predict both MS and cognitive status. Specifically, people with MS

showed higher average controllability, lower modal controllability, and lower activation

energy in the thalamus. Thalamic network controllability measures proved more effective

than thalamic volume alone in distinguishing MS from healthy controls, and in predicting

cognitive status. Overall, this study reveals potential mechanisms by which MS-related

changes in resting-state functional connectivity impair the thalamus' ability to drive brain

state dynamics, and contribute to cognitive impairment in MS.

The observed changes in network controllability in this work align with previous

studies reporting changes in brain activity dynamics in MS.[5,25,30] The present work, however,

extends prior studies by elucidating potential mechanisms through which MS pathology

disrupts brain activity dynamics. The controllability measures used in this study provide a

holistic view of how specific brain regions drive both subtle and dramatic shifts in cognitive

and neural states. Specifically, average controllability measures how easily a brain region

move the brain into nearby or easily reachable states, which reflects the brain capacity for

low-energy-cost and frequent small adjustments in brain states.[17–19] Modal controllability, on

the contrary, measures a region's ability to move the brain into difficult or unstable states,

which is important for executing high-energy-cost large transitions in brain activity (e.g.

between resting and active states).[17–19] Regional activation energy captures the feasibility or

minimum energy required by the given region to induce a transition between brain states.[17–19]

The directions of the observed controllability changes followed a consistent pattern (e.g.

increased average controllability, decreased modal controllability, and decreased activation

energy), regardless of whether we examined all cortical regions or specific cortical or

subcortical nodes. This implies that MS pathology does not induce random changes in brain

activity transitions; instead, it produces a disease-related pattern across the brain, consistently

characterized by greater difficulties in supporting high-, as opposed to low-energy-cost

transitions.

Our results revealed a selective involvement in controllability changes in MS, wherein

the subcortical network and particularly the thalamus exhibited the most pronounced changes

among the whole brain. A previous controllability study in healthy people found that the

subcortical network showed the most imbalance between average controllability and modal

controllability - it contributed the most to low-energy-cost state transitions (highest average

controllability) while the least to high-energy-cost state transitions (lowest modal

controllability).[19] The healthy cohort in our study conformed to that pattern. However

interestingly, MS pathology seems to exacerbate this imbalance in the subcortical network,

that is, in MS, the highest average controllability further increased, while the lowest modal

controllability further decreased. A recent study in healthy people observed higher average

controllability at resting state while higher modal controllability during cognitive tasks.[31]

This was interpreted as the resting state being a 'ground state' that maintains the energy cost

at a relatively low level, whereas performing cognitive tasks represents an 'excited state' that

consumes a large amount of energy to facilitate cognitive functions.[31] Given that the

subcortical network, particularly the thalamus, is one of the most vulnerable brain areas

affected by MS,[6–8,10–15,32–34] the controllability imbalance might be a manifestation of disease

attacks in these areas. This provides a potential mechanism explaining increased cognitive

impairment with disease progression. The thalamus increasingly 'drives' the brain transitions

towards low-energy-cost states (like the resting state) while relinquishing transitions towards

high-energy-cost states (like the cognitive task state). This process might help preserve

fundamental neural activities against disease attacks but, on the other hand, impact brain
functioning associated with high-energy-cost activities, typically cognitive processes.

The analysis of cognitive subgroups further supported this view that thalamic
controllability changes may impact cognitive performance in patients. While both CIMS and
CPMS showed controllability changes compared to HC, CIMS exhibited significantly greater
changes in the thalamus than CPMS. This indicated that CIMS experiences greater difficulty
in the thalamus supporting brain transitions towards difficult-to-reach states, which are
typically associated with high-energy-cost cognitive functions.[17–19,31] As a key hub with
strong connections across the brain and with known roles in cognition (e.g. the anterior
thalamic nuclei is critical for memory), thalamic damage has received considerable attention
in MS as a predictor of cognitive impairment.[6–8,34] Several studies converge to show that the
thalamus is an early site of pathology in MS,[11–13] while its structure and function have been
reported to determine the severity of cognitive impairment in patients.[7,35] These findings
strongly suggest thalamic changes as promising biomarkers for cognitive dysfunction in MS.
However, a key question would be: how does MS pathology progress from only localized
damage in thalamus (and a few neighbouring regions) in the early disease phase[11–16,36]
towards the widespread 'network collapse' across the brain in the late disease phase,[16,36,37]
culminating in cognitive dysfunction. The present study considering control processes from a
bioengineering perspective sheds lights on this. Recent evidence showed that CIMS,
compared to CPMS, required more control energy to transition between brain states.[25] In light
of this evidence, our findings suggest that early disease attacks produce a shift in
controllability in the thalamus that promotes brain network changes towards low-energy-cost
activity patterns, which would preserve energy for essential neural activities. However, this
'energy-saving' mode restricts the brain's efficiency to support high-energy-cost cognitive
functions in patients, gradually leading to impaired performance in cognitive functions. This
highlights a potential pathobiological mechanism linking thalamic changes to cognitive
impairment in MS.

Our results demonstrate that thalamic network controllability can help distinguish MS
patients from healthy controls and differentiate between patients with different level of
disability and cognitive impairment, with better performance compared to previously
reported classification analysis in this disease.[38] While both thalamic volume and
controllability contribute to classifying patients with different levels of disability, only
thalamic controllability achieves high classification performance in distinguishing between
CIMS and CPMS. These findings suggest that thalamic controllability offers complementary

information to volumetric measures in distinguishing patient groups. In particular,

controllability appears to be more specifically associated with cognitive impairment, rather

than just reflecting a general marker of network collapse. Importantly, the mechanistic

interpretation of controllability changes potentially allows for explainable diagnosis. This is a

key advantage compared to typical diagnostic tools based on statistical classification, which

only allows for a yes or no answer.

Notably, a recent longitudinal study in MS reported that volume changes in deep grey

matter regions, including the thalamus, were correlated with worsening clinical disability

over the course of the disease.[32] In parallel, altered functional dynamics in the subcortical

areas, particularly a hyperflexible reorganization of brain activity, have also been observed in

MS, showing significant associations with the development of clinical impairment.[39] These

findings underscore the potential importance of the dynamic profiles of subcortical regions,

like the thalamus, in understanding the progression of clinical dysfunctions in MS. Emerging

evidence highlights a complex and dynamic interplay between cognitive impairment,

physical disability progression, and thalamic structural and functional changes in MS.

Longitudinal studies have demonstrated that cognitive impairment at diagnosis can serve as a

predictor of subsequent disability milestones, including faster physical decline and poorer

clinical outcomes.[40–42] Likewise, thalamic structural and functional changes at baseline has

been shown to predict not only future cognitive dysfunctions but also worsening disability,

underlining the thalamus as a central region implicated in broader neurodegenerative

processes in MS.[6–8] Conversely, individuals with more severe disability tend to exhibit

greater degrees of cognitive dysfunction and more pronounced thalamic alterations.[43] These

findings suggest that cognitive impairment, thalamic changes, and clinical disability may not

occur in isolation but rather reflect shared pathological pathways or processes. Taken together,

the above evidence supports the hypothesis that changes in thalamic controllability may serve

as an early biomarker of cognitive decline and potentially contribute to the progression of

cognitive dysfunction in MS. Future longitudinal studies tracking network controllability

alongside cognitive outcomes in MS will be essential to formally test this hypothesis.

This study has several limitations. First, although the CIMS and CPMS groups did not

differ significantly in age or sex, the overall MS group was older than the healthy control

group. To mitigate the potential influence of these demographic differences on our findings,

we included age and sex as covariates in all relevant statistical models. Second, the imaging

scanning parameters and cognitive assessments differed between the two independent

datasets. However, the observed similar pattern of results demonstrates the robustness of the

findings despite these differences in acquisition and scanner between datasets. Future studies with multiple MS cohorts using paired scanning parameters and cognitive assessments are warranted to better replicate the controllability changes in patients with different cognitive statuses. Third, our study is cross-sectional; further longitudinal studies are needed to determine how network controllability develops with disease progression in MS.

Conclusion

This study moves beyond confirming thalamic changes in MS by characterizing how the MS-related damage significantly impact the thalamus ability to drive brain-wide dynamic activity, and how this helps explain cognitive impairment in this condition. Our results demonstrate that the thalamus in cognitively impaired MS patients is less able to facilitate brain transitions crucial for high-energy-cost cognitive functions, providing novel insights into the pathological mechanisms linking thalamic functional changes to cognitive impairment in MS.

Data and Code Availability

The data and code that support the results of this study are available from the corresponding author upon reasonable request and with permission.

Author Contributions

Y.L., N.T.B., and N.M. contributed to the conception and design of the study. I.L., Y.L., N.T.B., and N.M. contributed to the acquisition of data. Y.Y., A.W., Z.Z., M.C.L., N.T.B., and N.M. contributed to analysis or interpretation of data. Y.Y., A.W., V.T., Y.L., N.T.B., and N.M. contributed to drafting/revision of the manuscript.

Declaration of Competing Interests

Y.Y., A.W., I.L., Z.Z. and M.C.L. report no disclosures. V.T. reports consulting fees from Novartis, Janssen, Alexion, Biogen, Lundbeck, Almirall and Viatris; payments from Novartis, Janssen, Alexion, Biogen, Merck, Lundbeck, Almirall, Roche, Bristol Myers Squibb, Viatris, Horizon and Sanofi; and research grants from the MS Society UK. Y.L. reports no disclosures. N.T.B. reports research grants from the Medical Research Council UK (MR/X005267/1) during the conduct of the study.

Acknowledgements

This work was funded by research grants from the MS Society UK and MRC UK (MR/X005267/1). We extend our gratitude to Dr. Danka Jandric, Dr. Elizabeth McManus, Jessica Haigh, Megan Sheppard, Katie Moran, Rose-Marie Kouwenhoven, and all our colleagues from the MISC and NIMO labs for their kind support throughout this study.

Supplementary Material

Supplementary materials are available online.

References

1. Chiaravalloti ND, DeLuca J. Cognitive impairment in multiple sclerosis. 2008;7:13.

2. Eijlers AJC, Wink AM, Meijer KA, Douw L, Geurts JJG, Schoonheim MM. Reduced Network Dynamics on Functional MRI Signals Cognitive Impairment in Multiple Sclerosis. *Radiology*. 2019;292(2):449-457. doi:10.1148/radiol.2019182623

3. Meijer KA, Eijlers AJC, Douw L, et al. Increased connectivity of hub networks and cognitive impairment in multiple sclerosis. *Neurology*. 2017;88(22):2107-2114. doi:10.1212/WNL.0000000000003982

4. Jandric D, Lipp I, Paling D, et al. Mechanisms of Network Changes in Cognitive Impairment in Multiple Sclerosis. *Neurology*. 2021;97(19):e1886-e1897. doi:10.1212/WNL.0000000000012834

5. d'Ambrosio A, Valsasina P, Gallo A, et al. Reduced dynamics of functional connectivity and cognitive impairment in multiple sclerosis. *Mult Scler*. 2020;26(4):476-488. doi:10.1177/1352458519837707

6. Tona F, Petsas N, Sbardella E, et al. Multiple sclerosis: altered thalamic resting-state functional connectivity and its effect on cognitive function. *Radiology*. 2014;271(3):814-821. doi:10.1148/radiol.14131688

7. Schoonheim MM, Hulst HE, Brandt RB, et al. Thalamus structure and function determine severity of cognitive impairment in multiple sclerosis. *Neurology*. 2015;84(8):776-783. doi:10.1212/WNL.0000000000001285

8. Carotenuto A, Valsasina P, Hidalgo de la Cruz M, et al. Divergent time-varying connectivity of thalamic sub-regions characterizes clinical phenotypes and cognitive status in multiple sclerosis. *Mol Psychiatry*. 2022;27(3):1765-1773. doi:10.1038/s41380-021-01401-w

9. Yang Y, Li J, Li T, et al. Cerebellar connectome alterations and associated genetic signatures in multiple sclerosis and neuromyelitis optica spectrum disorder. *J Transl Med*. 2023;21(1):352. doi:10.1186/s12967-023-04164-w

10. Jandric D, Doshi A, Scott R, et al. A Systematic Review of Resting-State Functional MRI Connectivity Changes and Cognitive Impairment in Multiple Sclerosis. *Brain Connectivity*. Published online 2022:brain.2021.0104. doi:10.1089/brain.2021.0104

11. Coupé P, Planche V, Mansencal B, et al. Lifespan neurodegeneration of the human brain in multiple sclerosis. *Human Brain Mapping*. 2023;n/a(n/a). doi:10.1002/hbm.26464

12. Eshaghi A, Marinescu RV, Young AL, et al. Progression of regional grey matter atrophy in multiple sclerosis. *Brain*. 2018;141(6):1665-1677. doi:10.1093/brain/awy088

13. Tozlu C, Olafson E, Jamison KW, et al. The sequence of regional structural disconnectivity due to multiple sclerosis lesions. *Brain Communications*. 2023;5(6):fcad332. doi:10.1093/braincomms/fcad332

14. Azevedo CJ, Cen SY, Khadka S, et al. Thalamic atrophy in multiple sclerosis: A magnetic resonance imaging marker of neurodegeneration throughout disease. *Annals of Neurology*. 2018;83(2):223-234. doi:10.1002/ana.25150

15. Fleischer V, Ciolac D, Gonzalez-Escamilla G, et al. Subcortical Volumes as Early Predictors of Fatigue in Multiple Sclerosis. *Annals of Neurology*. 2022;91(2):192-202. doi:10.1002/ana.26290

16. Schoonheim M. Collapsing networks: new avenues for functional connectivity analyses in multiple sclerosis. *Swiss Arch Neurol Psychiatr Psychother*. Published online May 30, 2020. doi:10.4414/sanp.2020.03110

17. Lynn CW, Bassett DS. The physics of brain network structure, function and control. *Nat Rev Phys*. 2019;1(5):318-332. doi:10.1038/s42254-019-0040-8

18. Gu S, Pasqualetti F, Cieslak M, et al. Controllability of structural brain networks. *Nat Commun*. 2015;6(1):8414. doi:10.1038/ncomms9414

19. Deng S, Li J, Thomas Yeo BT, Gu S. Control theory illustrates the energy efficiency in the dynamic reconfiguration of functional connectivity. *Commun Biol*. 2022;5(1):295. doi:10.1038/s42003-022-03196-0

20. Bernhardt BC, Fadaie F, Liu M, et al. Temporal lobe epilepsy: Hippocampal pathology modulates connectome topology and controllability. *Neurology*. 2019;92(19). doi:10.1212/WNL.0000000000007447

21. Zarkali A, McColgan P, Ryten M, et al. Differences in network controllability and regional gene expression underlie hallucinations in Parkinson's disease. *Brain*. 2020;143(11):3435-3448. doi:10.1093/brain/awaa270

22. Hahn T, Winter NR, Ernsting J, et al. Genetic, individual, and familial risk correlates of brain network controllability in major depressive disorder. *Mol Psychiatry*. Published online January 13, 2023. doi:10.1038/s41380-022-01936-6

23. Li Q, Yao L, You W, et al. Controllability of Functional Brain Networks and Its Clinical Significance in First-Episode Schizophrenia. *Schizophrenia Bulletin*. 2023;49(3):659-668. doi:10.1093/schbul/sbac177

24. Parkes L, Moore TM, Calkins ME, et al. Network controllability in transmodal cortex predicts positive psychosis spectrum symptoms. *Biol Psychiatry*. 2021;90(6):409-418. doi:10.1016/j.biopsych.2021.03.016

25. Broeders T a. A, Dam M van, Pontillo G, et al. Energetically costly functional network dynamics in cognitively impaired multiple sclerosis patients. Published online April 22, 2024:2024.04.21.24306140. doi:10.1101/2024.04.21.24306140

26. Sepulcre J, Vanotti S, Hernández R, et al. Cognitive impairment in patients with multiple sclerosis using the Brief Repeatable Battery-Neuropsychology test. *Mult Scler*. 2006;12(2):187-195. doi:10.1191/1352458506ms1258oa

27. Schaefer A, Kong R, Gordon EM, et al. Local-Global Parcellation of the Human Cerebral Cortex from Intrinsic Functional Connectivity MRI. *Cerebral Cortex*. 2018;28(9):3095-

3114. doi:10.1093/cercor/bhx179

28. Tian Y, Margulies DS, Breakspear M, Zalesky A. Topographic organization of the human subcortex unveiled with functional connectivity gradients. *Nat Neurosci*. 2020;23(11):1421-1432. doi:10.1038/s41593-020-00711-6

29. Yeo BTT, Krienen FM, Sepulcre J, et al. The organization of the human cerebral cortex estimated by intrinsic functional connectivity. *Journal of Neurophysiology*. 2011;106(3):1125-1165. doi:10.1152/jn.00338.2011

30. Romanello A, Krohn S, von Schwanenflug N, et al. Functional connectivity dynamics reflect disability and multi-domain clinical impairment in patients with relapsing-remitting multiple sclerosis. *NeuroImage: Clinical*. 2022;36:103203. doi:10.1016/j.nicl.2022.103203

31. Deng S, Gu S. Controllability Analysis of Functional Brain Networks. Published online March 18, 2020. doi:10.48550/arXiv.2003.08278

32. Eshaghi A, Prados F, Brownlee WJ, et al. Deep gray matter volume loss drives disability worsening in multiple sclerosis. *Ann Neurol*. 2018;83(2):210-222. doi:10.1002/ana.25145

33. Mahajan KR, Nakamura K, Cohen JA, Trapp BD, Ontaneda D. Intrinsic and Extrinsic Mechanisms of Thalamic Pathology in Multiple Sclerosis. *Ann Neurol*. 2020;88(1):81-92. doi:10.1002/ana.25743

34. Houtchens MK, Benedict RHB, Killiany R, et al. Thalamic atrophy and cognition in multiple sclerosis. *Neurology*. 2007;69(12):1213-1223. doi:10.1212/01.wnl.0000276992.17011.b5

35. Lorefice L, Carta E, Frau J, et al. The impact of deep grey matter volume on cognition in multiple sclerosis. *Multiple Sclerosis and Related Disorders*. 2020;45:102351. doi:10.1016/j.msard.2020.102351

36. Schoonheim MM, Broeders TAA, Geurts JJG. The network collapse in multiple sclerosis: An overview of novel concepts to address disease dynamics. *NeuroImage: Clinical*. 2022;35:103108. doi:10.1016/j.nicl.2022.103108

37. Schoonheim MM, Meijer KA, Geurts JJG. Network Collapse and Cognitive Impairment in Multiple Sclerosis. *Front Neurol*. 2015;6. doi:10.3389/fneur.2015.00082

38. Tozlu C. Larger lesion volume in people with multiple sclerosis is associated with increased transition energies between brain states and decreased entropy of brain activity.pdf. *Network Neuroscience*. Published online 2022. doi:https://doi.org/10.1162/netn_a_00292

39. von Schwanenflug N, Koch SP, Krohn S, et al. Increased flexibility of brain dynamics in patients with multiple sclerosis. *Brain Communications*. 2023;5(3):fcad143. doi:10.1093/braincomms/fcad143

40. Pitteri M, Romualdi C, Magliozzi R, Monaco S, Calabrese M. Cognitive impairment predicts disability progression and cortical thinning in MS: An 8-year study. *Mult Scler*. 2017;23(6):848-854. doi:10.1177/1352458516665496

41. Deloire M, Ruet A, Hamel D, Bonnet M, Brochet B. Early cognitive impairment in multiple sclerosis predicts disability outcome several years later. *Mult Scler*. 2010;16(5):581-587. doi:10.1177/1352458510362819

42. Moccia M, Lanzillo R, Palladino R, et al. Cognitive impairment at diagnosis predicts 10-year multiple sclerosis progression. *Mult Scler*. 2016;22(5):659-667. doi:10.1177/1352458515599075

43. Schoonheim MM, Pinter D, Prouskas SE, et al. Disability in multiple sclerosis is related to thalamic connectivity and cortical network atrophy. *Mult Scler*. 2022;28(1):61-70. doi:10.1177/13524585211008743

44. Xia M, Wang J, He Y. BrainNet Viewer: A Network Visualization Tool for Human Brain Connectomics. *PLOS ONE*. 2013;8(7):e68910. doi:10.1371/journal.pone.0068910

45. Wang J, Wang X, Xia M, Liao X, Evans A, He Y. GRETNA: a graph theoretical network analysis toolbox for imaging connectomics. *Front Hum Neurosci*. 2015;9. doi:10.3389/fnhum.2015.00386

Table 1. Demographic, clinical, and neuropsychological variables from the main dataset

	HC (n = 27)	MS (n = 102)	*p* value (HC vs MS)	CPMS (n = 47)	CIMS (n = 55)	*p* value (HC vs CPMS vs CIMS)
Age, y	37 (23-59)	45 (18-60)	0.012	42 (18-60)	47 (20-60)	0.012[b]
Sex, n (female/male)	15/12	69/33	0.241	36/11	33/22	0.108
Education, y	19 (12-30)	15 (10-30)	< 0.001	15 (10-27)	14 (10-30)	< 0.001[b, c]
Disease duration, y	-	12 (1-39)	-	12 (2-37)	11.5 (1-39)	0.794
Lesion load	-	9,137 (595-47,026)	-	9,008 (636-35,785)	9,407 (595-47,026)	0.340
EDSS	-	4.0 (0-6.5)	-	4.0 (0-6)	4.0 (0-6.5)	0.251
MSFC						
25-FWT	4.35 (3.20-5.40)	5.25 (3.60-26.80)	0.003	5.15 (3.70-12.95)	5.43 (3.60-26.80)	0.002[b]
9-HPT	18.65 (15.35-23.00)	21.75 (16.35-59.50)	< 0.001	21.45 (17.15-44.85)	21.95 (16.35-59.50)	< 0.001[a,b,c]
PASAT3	51.00 (35.00-59.00)	43.50 (0-60.00)	< 0.001	50.00 (30.00-60.00)	34.00 (0-58.00)	< 0.001[a,b]
BRB-N						
Verbal memory	36.33 (21.33-47.33)	29.17 (4.00-48.33)	0.002	36.00 (22.33-48.33)	23.00 (4.00-47.33)	< 0.001[a,b]
Visual memory	7.83 (4.50-9.50)	6.17 (2.67-9.67)	0.020	7.33 (4.67-9.67)	5.33 (2.67-9.33)	< 0.001[a,b]
Information processing, attention, executive function	50.67 (36.33-62.67)	41.83 (12.67-58.00)	< 0.001	46.67 (36.67-58.00)	34.67 (12.67-56.67)	< 0.001[a,b]
Verbal fluency	29.00 (13.00-44.00)	27.00 (7.00-42.00)	0.031	29.00 (19.00-42.00)	24.00 (7.00-40.00)	< 0.001[a,b]
Global BRB-N	33.78 (26.56-42.52)	27.85 (8.56-38.59)	< 0.001	32.74 (26.00-38.59)	23.62 (8.56-35.22)	< 0.001[a,b]

Data is represented as median (range) except for sex ratio (female/male). HC = healthy controls; MS = multiple sclerosis; CPMS = cognitively preserved
MS; CIMS = cognitively impaired MS; EDSS = Expanded Disability Status Scale; MSFC = Multiple Sclerosis Functional Composite; 25-FWT = 25 Foot
Walk Test; 9-HPT = 9 Hole Peg Test; PASAT3 = Paced Auditory Serial Addition Task 3 seconds. BRB-N = Brief Repeatable Battery of

Neuropsychological Tests.

[a] Significant difference between the CIMS and CPMS.

[b] Significant difference between the CIMS and HC.

[c] Significant difference between the CPMS and HC.

Table 2. Classification performance using different features

Features	AUC	Precision	Accuracy	Sensitivity	Specificity
MS vs. HC					
Thalamic controllability	80.1% (1.7%)	90.5% (1.4%)	74.5% (2.2%)	75.7% (2.3%)	70.0% (4.8%)
Thalamic volume	74.5% (0.9%)	88.8% (0.8%)	68.1% (1.3%)	68.3% (1.5%)	67.6% (2.6%)
Combination	88.3% (1.1%)	93.9% (1.1%)	80.9% (1.8%)	81.1% (1.8%)	80.2% (3.9%)
CIMS vs. CPMS					
Thalamic controllability	80.7% (2.2%)	75.4% (3.6%)	72.4% (3.1%)	72.7% (3.5%)	72.0% (5.1%)
Thalamic volume	38.2% (3.6%)	45.3% (3.8%)	41.6% (3.6%)	41.2% (5.1%)	42.1% (5.0%)
Combination	68.2% (2.5%)	64.6% (3.5%)	61.7% (3.4%)	64.5% (3.7%)	58.4% (5.9%)

577 Data is represented as mean (standard deviation). CPMS = cognitively preserved MS; CIMS = cognitively impaired MS; HC = healthy controls; MS =

578 multiple sclerosis

Mean time courses   **Functional connectivity**   **Network controllability**

Figure 1. Overview of network controllability calculation. Based on rs-fMRI data from

129 participants and using combined cortical and subcortical parcellations, we extracted

regional mean time courses and calculated functional connectivity between pairs of regions to

construct brain networks. We then calculated the most commonly used controllability

measures to quantify how specific regions influence brain activity transitions throughout the

brain. Specifically, average controllability measures how easily a brain region move the brain

into nearby or easily reachable states, which reflects the brain capacity for low-energy-cost

and frequent small adjustments in brain states. Modal controllability, on the contrary,

measures a region's ability to move the brain into difficult or unstable states, which is

important for executing high-energy-cost large transitions in brain activity (e.g. between

resting and active states). Regional activation energy captures the feasibility or minimum

energy required by the given region to induce a transition between brain states.

Figure 2. Controllability changes in the subcortical network in MS. Increased average controllability but decreased modal controllability and decreased activation energy in the subcortical network (averaged across the 54 subcortical ROIs) were observed in MS from the main dataset. Replicated increased average controllability in the subcortical network were observed in MS from the replication dataset. Brain network visualizations were generated using BrainNet Viewer[44] and GRETNA[45]. The nodes and edges illustrate the connections of subcortical regions with other parts of the brain. Specifically, the nodes represent the subcortical regions and the regions to which they are connected. The edges depict the top 200 connections with the highest functional connectivity strength among the whole brain connections. SubCor = subcortical network; $^{*}p < 0.05$, FDR corrected.

Figure 3. Controllability changes in the thalamus in MS. Increased average controllability but decreased modal controllability and decreased activation energy in the thalamus (averaged across the 16 thalamic ROIs) were observed in MS from the main dataset. Replicated increased average controllability in the thalamus were observed in MS from the replication dataset. Brain network visualizations were generated using BrainNet Viewer[44] and GRETNA[45]. The nodes and edges illustrate the connections of thalamic regions with other parts of the brain. Specifically, the nodes represent the thalamic regions and the regions to which they are connected. The edges depict the top 200 connections with the highest functional connectivity strength among the whole brain connections. SubCor = subcortical network; $^*p < 0.05$, FDR corrected.

Figure 4. Controllability changes in the subcortical network in CIMS and CPMS.

Increased average controllability but decreased modal controllability and decreased activation

energy in the subcortical network (averaged across the 54 subcortical ROIs) in both CIMS

and CPMS when compared to HC. Brain network visualizations were generated using

BrainNet Viewer[44] and GRETNA[45]. The nodes and edges illustrate the connections of

subcortical regions with other parts of the brain. Specifically, the nodes represent the

subcortical regions and the regions to which they are connected. The edges depict the top 200

connections with the highest functional connectivity strength among the whole brain

connections. SubCor = subcortical network; $^{*}p < 0.05$, FDR corrected.

Figure 5. Controllability changes in the thalamus in CIMS and CPMS. Both CIMS and

CPMS showed increased average controllability in the thalamus (averaged across the 16

thalamic ROIs) when compared to HC, while CIMS exhibited significantly greater changes

than CPMS. Besides, CIMS showed additional decreases in modal controllability and

activation energy in the thalamus compared to HC. Brain network visualizations were

generated using BrainNet Viewer[44] and GRETNA[45]. The nodes and edges illustrate the

connections of thalamic regions with other parts of the brain. Specifically, the nodes represent

the thalamic regions and the regions to which they are connected. The edges depict the top

200 connections with the highest functional connectivity strength among the whole brain

connections. SubCor = subcortical network; $^{*}p < 0.05$, FDR corrected.

Figure 6. Classification ROC curve derived from volumetric, controllability, combined, and random classifiers. In distinguishing MS from HC, classifiers based on the thalamic network controllability alongside thalamic volume achieved the best performance (AUC = 88.3%) among all the four types of classifiers. In distinguishing CIMS from CPMS, classifiers based on the thalamic network controllability measures alone achieved the best performance (AUC = 80.7%) among all the four types of classifiers. AUC = area under curve; ROC = receiver operating characteristic.