Brain-wide topographic coordination of traveling spiral waves

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Abstract

Traveling waves of activity are a prevalent phenomenon within neural networks of diverse brain regions and species[1–4], and have been implicated in myriad brain functions including sensory perception[5–8], memory[9], spatial navigation[10–12] and motor control[13,14]. However, the anatomical basis for these waves, and whether they are locally confined versus distributed across the brain, remains unclear. Here we use cortex-wide imaging and large-scale electrophysiology in awake mice to reveal the organization of traveling waves across spatial scales. Traveling waves formed spiral patterns predominantly centered on somatosensory cortex. Strikingly, the local axonal architecture of neurons in sensory cortex exhibited a matching circular arrangement. At the cortex-wide scale, these spiral waves were mirrored between hemispheres and between sensory and motor cortex, reflecting topographic long-range axons. Finally, at the brain-wide scale, cortical spiral waves were coordinated with subcortical spiking patterns in the thalamus, striatum and midbrain. These results establish that traveling waves are structured by axonal pathways and globally impact neural activity across diverse brain systems.

Introduction

Spiral waves, also called vortices, are among the dynamic patterns of brain activity previously observed across various timescales and species including turtles[15], mice[16,17], rats[18] , monkeys[9] and humans[19–21]. These patterns, and associated traveling waves, are strongly correlated with a variety of perceptual, cognitive, and motor behaviors[5–14]. Previous studies of such waves often focused on measures of neural activity at low temporal[20,21] or spatial[5,9,19] resolutions, limiting their ability to link the organization of these dynamic patterns with underlying features of the neural architecture.

Moreover, prior studies of traveling waves in mammals have primarily focused on waves in isolated brain regions, especially neocortex[5,7,9,13–15,17–19,21], hippocampus[10–12], and others[8,22]. Despite the known anatomical[23–26] and functional connectivity [27–29] between the neocortex and the thalamus, basal ganglia, and midbrain, it remains unclear whether fast traveling waves, on the sub-second timescale of perception and action, are topographically coordinated in relation to

long-range connectivity in the adult brain[30–35]. The mere existence of axonal projections from one brain region to another does not imply that all patterns of activity are transmitted from one region to the other. Specifically, the particular neurons that project to the downstream region may not represent the traveling wave, or, traveling waves could be in the 'null space' of activity, that is, they could be patterns of activity that are not transmitted to target areas[36,37]. Therefore, establishing whether propagating waves of neural activity are globally distributed versus locally confined is a key, non-trivial step towards understanding the mechanisms of dynamic activity propagation in the mammalian brain.

Here, we used fast mesoscopic imaging with large-scale electrophysiology to elucidate the dynamic neuronal activity patterns of the mouse brain, the features of axonal architecture underlying them, and their coordination across diverse brain systems.

Results

Spiral waves in mouse cortex

To investigate the mesoscale spatiotemporal dynamics of neural activity across the cortex, we performed widefield calcium imaging in awake, head-fixed mice expressing either GCaMP7 in excitatory neurons or GCaMP8 in all neurons. We focused our analysis on the 2-8 Hz frequency range, and observed prominent activity in this range across the dorsal cortex during quiet wakefulness states, with the highest power in the retrosplenial cortex (Extended Data Fig.1). Activity in this frequency range includes an alpha-like 3-6 Hz oscillation in visual cortex[38–40] which is correlated with perceptual sensitivity in discrimination tasks[41], and may include homologues of the human somatosensory mu rhythm[42]. To visualize the spatiotemporal propagation of traveling waves in this frequency range, we applied the Hilbert transform to the filtered data for each pixel independently to extract the oscillation phase at each moment in time (Fig.1a).

We consistently observed spiral waves, which exhibited a circular arrangement of oscillation phases, in the widefield imaging data (Fig.1a-c, Extended Data Fig.1; Video1). To characterize their properties, we designed an automated spiral detection algorithm (Extended Data Fig.2). To determine whether observed spirals occurred more frequently than expected by chance, we constructed 3D surrogate data with a Fourier phase shuffling method, in which the spatial and temporal autocorrelations of the data were preserved (Methods). While small spirals commonly occurred by chance in the shuffled data, large spirals (radius >= 40 pixels, or 0.69 mm) occurred in the original data significantly more often than in the shuffled data across sessions (n= 15 mice) and were therefore included for further analysis (Extended Data Fig.3). Spirals formed sequences persisting for tens to hundreds of milliseconds (Fig. 1b, d). Since single-frame spirals occurred frequently by chance in permuted data (Fig. 1d; Methods), we further focused analyses on spiral sequences lasting multiple sampling frames (>=57 ms; Fig.1d). Spiral waves with similar characteristics were also observed in LFP activity in wild type mice (Extended Data Fig.4), indicating that they did not arise from any artifact of calcium imaging. Spirals were also

observed in mice that expressed calcium-sensitive fluorescent proteins only in neuron somas and proximal dendritic segments (Extended Data Fig.5), indicating that they reflected patterns of local activity rather than axonal inputs.

The spiral activity patterns we observed were consistently localized, frequently occurring, and had a characteristic rotational speed. The majority of spiral waves swept across the somatotopic maps of the mouse body representation sequentially, including lower limb, upper limb, mouth, nose and the barrel field (Fig 1a-c, Extended Data Fig.1). Spiral centers were highly concentrated in the middle of primary somatosensory cortex (SSp) across animals (Fig 1e), a property observed across different mouse lines (Extended Data Fig.5), spiral sizes, and durations (Extended Data Fig.6). Spirals had a peak rate of 1.2 spirals/(mm^2*s) on average, or 3.4% of frames/mm^2 at 35 Hz (Fig.1e, Extended Data Fig.5, n= 15 mice). Spiral centers often drifted within a spiral sequence and were slightly more likely to rotate counterclockwise in the right hemisphere (Extended Data Fig.7). Spirals were more prevalent during high 2-8 Hz power, but were similarly prevalent when subjects were active or quiescent (Extended Data Fig.8). Spiral waves had consistent angular speed (ω) across different radii (31.9 ± 6.1 rad/s, mean ± STD, equivalent to 5.1 ± 1.0 Hz; Fig.1f, Extended Data Fig.9) but increasing linear speed as a function of radius (Fig. 1g, Extended Data Fig.9). The propagation speeds of these waves are therefore substantially slower than axonal conduction velocities, which are on the order of 0.5 m/s for lateral axons in rodent neocortex[43].

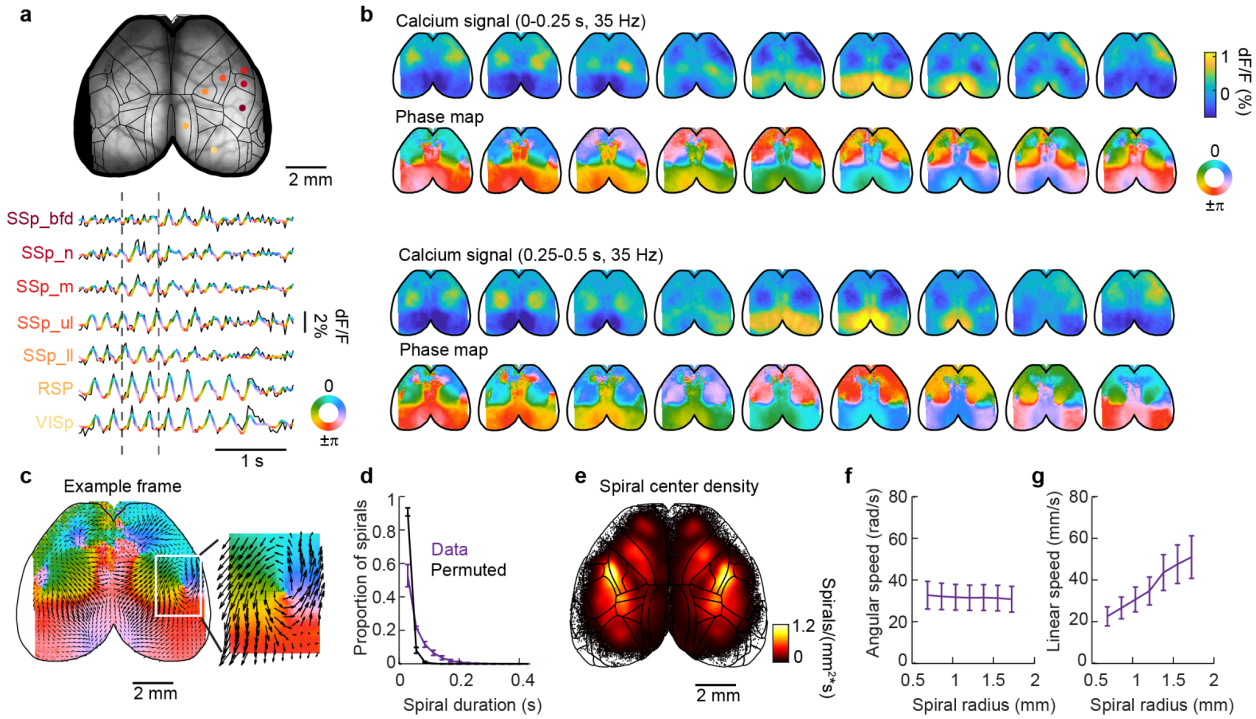

Figure 1. Spiral waves are prevalent in the neural dynamics of mouse cortex. a, Example activity traces from calcium imaging of the dorsal cortical surface. Raw traces (black) are overlaid with 2-8 Hz filtered traces color coded by phase values after the Hilbert transform. **b**, 18 example consecutive frames (0.5 second) of calcium signal maps and phase maps, within the window indicated by the dashed lines in panel **a**. **c**, Phase map from an example frame with spiral in the right hemisphere, and optical flow overlaid depicting wave direction. **d**, Durations of spirals in data (purple) and in permuted data (black). Error bar: standard error of the mean (n = 15 mice). **e**, Density estimate of spiral center distribution after automated spiral detection algorithm (n = 15 mice). **f**, Angular speed distribution as a function of spiral radius across 15 mice. **g**, Linear speed of spirals as a function of spiral radius. Abbreviations: SSp_bfd (primary somatosensory area, barrel field); SSp_n (primary somatosensory area, nose); SSp_m (primary somatosensory area, mouth); SSp_ll (primary somatosensory area, lower limb); SSp_ul (primary somatosensory area, upper limb); RSP (retrosplenial cortex); VISp (primary visual cortex).

An axonal basis for spirals in sensory cortex

To investigate the anatomical basis for the propensity of spirals to form around the somatosensory cortex, we examined the local axonal architecture of neurons in sensory cortex. Using an open dataset of cortical neuron reconstructions[44], we discovered that local axons from mouse cortical neurons are also organized circularly (Fig.2a-c). In particular, the major axes of the axonal terminals from single neurons exhibited a strong tendency to align perpendicular to the vector from the SSp center to the soma location (Fig. 2e; 87.4°, n = 435 neurons; 95% confidence interval for circular t-test = 82.8°-92°, $p < 0.05$; real data vs permutation distribution: $p < 0.05$, Watson's U^2 test). Moreover, the orientation of these axonal axes matched the propagation directions of spiral waves, exceeding a permuted distribution of flow vectors (Fig. 2d,f; see Methods; $p = 0.004$, student's t-test). A computational simulation of activity

propagation over sheets of cortical neurons, modeled as coupled oscillators with circularly biased connectivity as in the data, exhibited strengthened spiral dynamics relative to a model with isotropic connectivity (Extended Data Fig.10). The anatomical architecture of axons in the somatosensory cortex therefore corresponds to the spiral waves we observed, and could support the occurrence of these dynamic patterns.

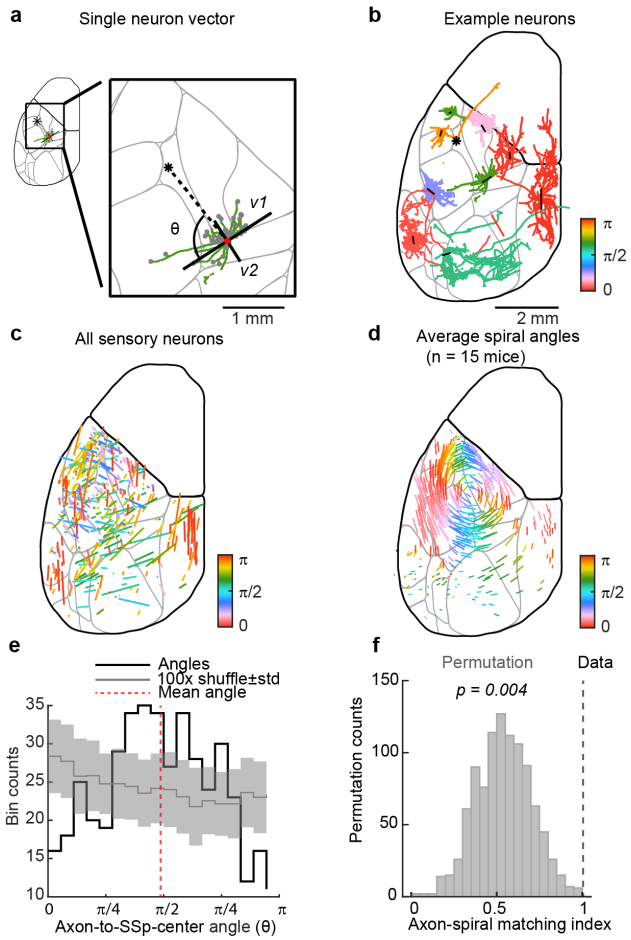

Figure 2. Axon orientations of single neurons match the circular arrangement of spiral waves around the middle of somatosensory cortex. a, Morphology of an example neuron's axonal arbor (green) with local axon terminals overlaid (gray). The top two singular vectors of the terminal point cloud (*v1*, *v2*; black) are overlaid on top of the axonal arbor and centered on the soma (red). Asterisk represents the middle of SSp, within the unassigned SSp (SSp-un) zone. Axon-to-SSp-center angle (θ) is the angle between the first singular vector (*v1*) and the vector from the soma to the SSp middle. **b**, Axonal arbors of 9 example neurons. The direction of the vector overlaid on top of the arbor (black) represents the first singular vector of the axon terminal cloud. The length of the vector represents axonal arbor polarity, which is the ratio between the first two singular values, with longer length indicating higher polarity. The vectors are centered on the cell soma positions. **c**, Axon orientation and polarity for all sensory neurons (n = 435 neurons), as in **b**. Color represents the angle of the vectors. **d**, Mean activity flow vectors of a collection of large spirals with the same direction of rotation across mice (n = 15). **e**, Histogram of axon-to-SSp-center angle (θ) for all 435 neurons. The mean angle across all neurons is indicated by the dashed red line. Mean and standard deviation of shuffled distribution is indicated in gray. **f**, Axon-flow matching index is significantly greater than the permuted distribution of flow vectors.

Topographically mirrored spirals across cortex

Spirals were often symmetrical between left and right hemispheres, as well as between sensory and motor cortex, divided along the border of primary somatosensory cortex (SSp) and primary motor cortex (MOp). When 2 spirals were detected simultaneously in neighboring mirrored brain structures at the same time (SSp-MOp, SSp-left-right, MOp-left-right), spirals were mostly traveling in the opposite direction (Fig.3a; full comparison, Extended Data Fig.7).

With the observation of cortical phase map symmetry along the border of SSp and MOp (Fig.1b, Fig.3a), we sought to look for the basis of spiral symmetry with functional connectivity. We used a reduced rank regression model to (1) predict activity in the right hemisphere from the left hemisphere or (2) predict activity in the sensory cortex from the motor cortex, divided along the border of SSp and MOp (Fig.3b). Reduced-rank regression analysis achieved 98 ± 0.1% (mean ± SEM, 15 mice) cross-validated variance explained with 16 latent reduced-rank components for both left-to-right and motor-to-sensory predictions (Fig.3c). As a result, neural activity of a given pixel in one hemisphere (or sensory cortex) can be fully represented as a linear combination of neural activity in the other hemisphere (or motor cortex) with its own unique and spatially localized kernel map, i.e., weight matrix (Fig.3d-g). Therefore, moment-to-moment population activity information is topographically shared between hemispheres, as well as between the sensory and motor cortex.

The spatial arrangement of the localized kernel maps closely matched the axonal projection maps across hemispheres (Fig.3h, Extended Data Fig.11), significantly exceeding scrambled axonal distribution (Fig.3i; kernel-axon matching index for real data: 1; 1000x permutation index: 0.3 ± 0.005, mean ± SEM; $p = 1.1 \times 10^{-5}$; Student's t-test; Methods). The same matching patterns were observed between activity kernel maps and axon projection maps between sensory and motor cortex (Fig.3j,k, Extended Data Fig.11; kernel-axon matching index for real data: 1; 1000x permutation index: 0.4 ± 0.01, mean ± SEM; $p = 0.001$; Student's t-test).

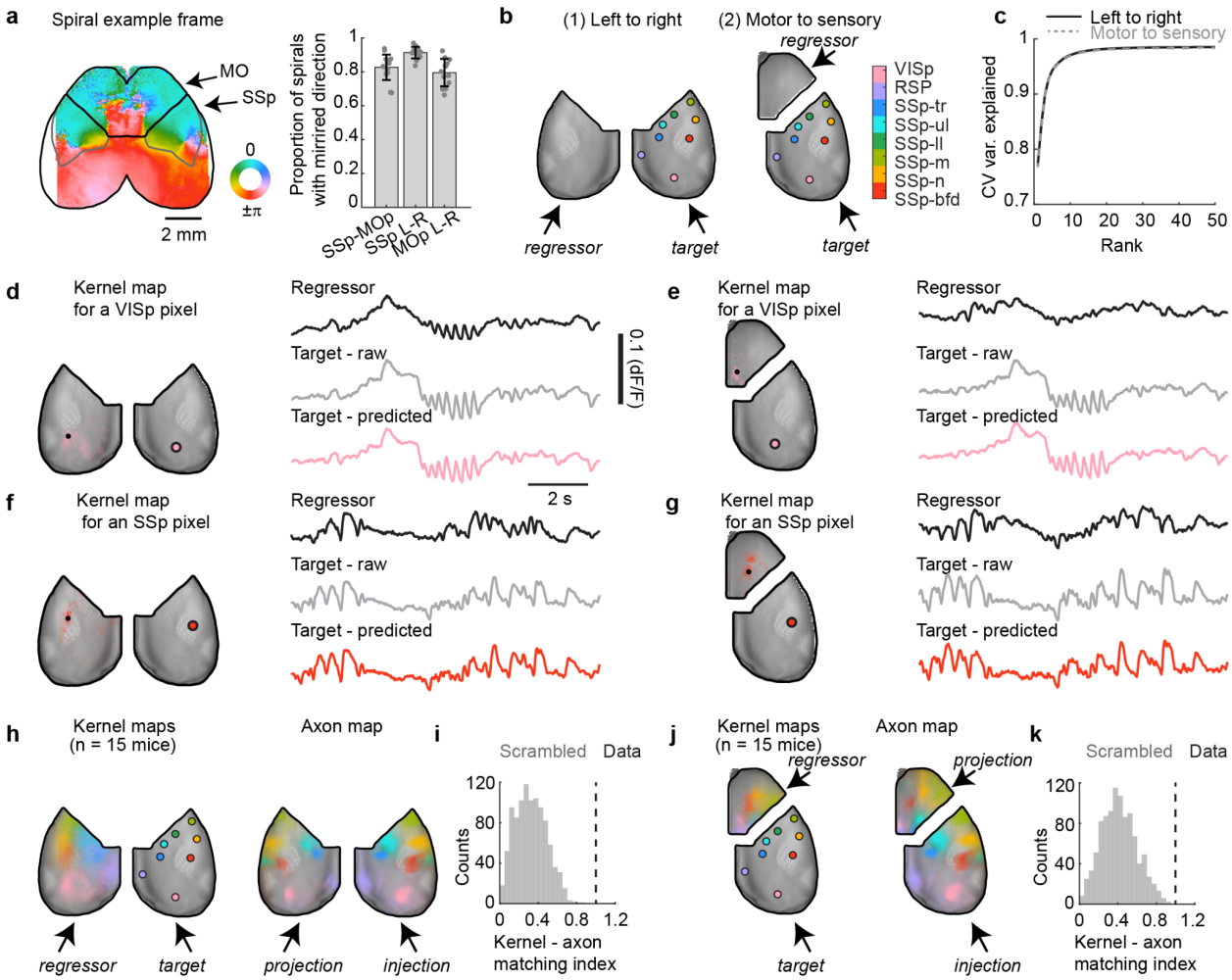

Figure 3. Spirals are mirrored between left and right hemispheres, and between sensory and motor cortex, reflecting an underlying topographic mapping of activity and long-range axons. a, Left: an example phase map with SSp/MOp border depicted in black outline. Right: proportion of paired spirals with mirrored direction between topographically connected cortical regions, including SSp versus MOp on the same hemisphere, SSp on left versus right hemispheres (SSp L-R), and MOp on left versus right hemisphere (MOp L-R). **b**, Schematic of regressions to predict right sensory cortical activity from (1) left sensory cortex and (2) right hemisphere motor cortex. Centers of 8 sensory cortical regions are highlighted in colored dots. **c**, Variance explained plateaued with around 16 latent components with Reduced Rank Regression, for both left-to-right prediction and motor-to-sensory prediction. **d**, Left: regression kernel map in the left hemisphere for predicting an example right VISp pixel. The "kernel map" is a visualization of the predictor weights with each pixel's color transparency scaled by the value of the weight matrix. Right: example regressor trace (black) with the highest value in the weight matrix from left hemisphere (top right); raw (gray, middle right) and predicted activity trace (pink, bottom right) of the example right VISp pixel. **e**, Same as **d**, but with motor cortex as regressor. **f**,**g**, Same as **d**,**e**, but for predicting an SSp-bfd pixel in the same time epoch as **d**,**e**. **h**, Left: averaged kernel maps for all example pixels in the right sensory cortex across 15 mice. Right: Axon targets in the left hemisphere from viral injections in the right hemisphere[25]. **i**, Topographic kernel-axon matching index, measuring how similar the axon projection fields are to the kernel maps, is significantly greater than the distribution of the index when permuting the injection identities. **j**,**k**, Same as **h**,**i**, but for activity kernels of motor-to-sensory prediction and axon targets in the motor cortex from the same viral injections as in **h**.

Brain-wide coordination of spiral waves

To investigate whether individual spiral waves simultaneously occur in cortex and in subcortical areas, we combined widefield imaging in the cortex with 4-shank Neuropixels electrophysiology in subcortical areas, including thalamus, striatum and midbrain (Fig.4a). When 2-8 Hz oscillation was prominent in the cortex, we consistently observed corresponding oscillations in the subcortical spiking activity (Fig.4b,c, Extended Data Fig.12). To test whether subcortical spiking activity contains information about cortical spiral wave propagation, we implemented a linear regression model to predict cortical activity from subcortical spiking activity. Subcortical spiking could predict cortical activity well across much, but not all, of the cortical surface (Fig.4c, Extended Data Fig.13), presumably because the subcortical regions were incompletely sampled.

We assessed whether spirals were present in the activity patterns of subcortical areas by asking whether predictions from subcortical activity recapitulated spirals in the cortical activity (Fig.4d,e, Extended Data Fig.12). We computed the probability that spirals in the raw frames rotated in the same direction as spirals in the predicted frames from all thalamic, stiatal and midbrain recordings sessions (Fig.4f). Spirals were significantly more likely to match rotation directions in the real spiking data compared to data in which neuron identities were shuffled, and the matching probability was above chance level (thalamus: 0.57 ± 0.01 vs 0.5 ± 0.01, $p = 3.8\text{x}10^{-4}$; striatum: 0.57 ± 0.02 vs 0.52 ± 0.01, $p = 0.03$; midbrain: 0.56 ± 0.02 vs 0.52 ± 0.02, $p = 0.04$; mean ± SEM; paired Student's t-test) for all subcortical regions (Fig.4g).

To determine whether traveling waves were more generally coordinated outside of spirals, we quantified waves with optical flow and compared them between raw and predicted cortical activity (Fig.4d,e, Extended Data Fig.12). Firstly, as cortical 2-8 Hz oscillation amplitude increased, phase maps were more likely to match for raw cortical activity and predicted activity from all subcortical regions across sessions (Fig.4h; thalamus: $p = 6\text{x}10^{-20}$; striatum: $p = 1\text{x}10^{-6}$; midbrain: $p = 2\text{x}10^{-4}$; main effect of 2-8 Hz amplitude, unbalanced two-way ANOVA). Moreover, as cortical 2-8 Hz oscillation amplitude increased, traveling wave directions were also more likely to match for cortical activity and predicted activity from all subcortical regions (Fig.4i; thalamus: $p = 3\text{x}10^{-15}$; striatum: $p = 5\text{x}10^{-4}$; midbrain: $p = 1\text{x}10^{-3}$; main effect of 2-8 Hz amplitude, unbalanced two-way ANOVA). Probability of wave matching significantly exceeded shuffled permutation for the majority of single sessions (Extended Data Fig.13; 10/10 sessions in thalamus, 12/12 sessions in stratum and 6/7 sessions in midbrain; unbalanced two-way ANOVA) and across sessions (Fig.4i; thalamus: $p = 1\text{x}10^{-16}$; striatum: $p = 2\text{x}10^{-6}$; midbrain: $p = 1\text{x}10^{-6}$; unbalanced two-way ANOVA). Therefore, cortical spirals and traveling waves are represented in subcortical brain areas on a moment-to-moment basis.

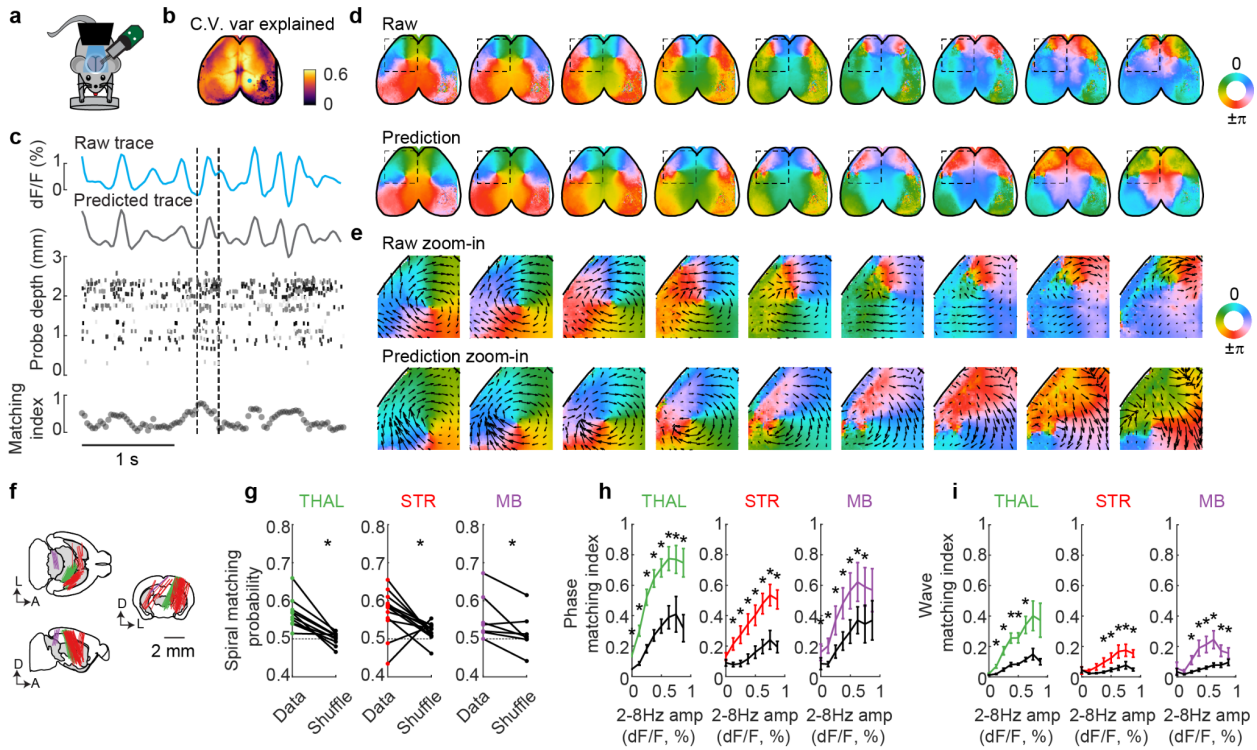

Figure 4. Spirals are coordinated between cortical and subcortical regions. a, Illustration of simultaneous cortical widefield and subcortical electrophysiological recordings with 4-shank Neuropixels 2.0 probes. **b**, Example map showing cross-validated variance explained of cortical widefield data predicted from thalamic population spiking. The craniotomy is in the right posterior cortex. **c**, Top: an example epoch of raw (blue) and predicted (gray) cortical calcium activity for an example pixel highlighted in **b**. Middle: thalamic spike raster plot, ordered by probe depth. The tips of the 4-shank probe were at 0 mm. Each neuron was color coded by a randomized shade of gray color. Bottom: Traveling wave matching index, comparing optical flow vectors between raw and predicted phase maps. **d**, Example raw (top) and predicted (bottom) phase maps of cortical activity within the dashed lines in **c**. **e**, Zoom-in of raw (top) and predicted (bottom) phase maps within the square ROI in **d**, with activity flow vectors overlaid. **f**, Probe trajectories were retrieved successfully in all 29 sessions (thalamus: 10, striatum: 12, midbrain 7). **g**, Spiral matching probabilities between spirals detected from raw and predicted cortical phase maps are above chance level (0.5), and are significantly greater than spiral matching probabilities from predictions with shuffled neuron identity across sessions. **h**, Predicted phase maps were more likely to match raw phase maps as 2-8 Hz amplitude increased. Phase matching indexes from subcortical spiking prediction were significantly higher than predictions from shuffled neuron identities. **i**, Direction of predicted traveling waves were more likely to match raw traveling waves as 2-8 Hz amplitude increased. Wave matching indexes were significantly higher than predictions from shuffled neuron identities.

Discussion

We observed spiral waves traveling across the somatotopic maps of the mouse sensorimotor cortex, matching a circular pattern of local axonal architecture. Spirals were also topographically mirrored between left and right cortical hemispheres, and between sensory and motor cortex, respecting long-range axonal connectivity. Spirals were widely distributed and coordinated across cortex, striatum, thalamus, and midbrain. These results establish that traveling waves in the mammalian brain are not a local phenomenon and therefore cannot be adequately understood by studying any one brain region in isolation.

In studying the 2-8Hz frequency range, we have not captured traveling wave dynamics on faster[5,9,45] or slower[20,21] timescales. Whether dynamics in those frequency ranges follow the same principles is an open question, as some evidence suggests that cortical activity in disparate frequency ranges may be uncoupled[46]. The spirals we observed were frequent but far from constant (peak density ~1.2 spirals/(mm^2*s)), so dynamics in other frequency ranges may dominate during time periods without spirals. Moreover, active behavioral engagement[9,21,47] and sensory stimulation[48,49] modulate cortical dynamics, so future studies may therefore investigate the influence of these factors on the dynamic patterns described here.

We found that spirals were centered in the middle of somatosensory cortex, an area of "unassigned" function in the Allen CCF ("SSp-un")[50] and unique in its poorly defined layer 4 compared to other somatosensory regions[51,52]. This region may therefore comprise a discontinuity or 'defect' in the cortical medium. Our findings show that cortical spirals are correlated with local axonal architecture, a generalization of prior observations of axonal orientation bias in the barrel cortex[53]. However, our data cannot disambiguate the direction of causality of this relationship, that is, whether the presence of circularly arranged axonal architecture drives spiral activity, or whether spiral activity patterns in this region drive the formation of this axonal architecture via plasticity mechanisms during development. Indeed, the observation of matching waves in three subcortical regions raises the possibility that the medium of wave propagation may not be limited to corticocortical connectivity. For example, thalamic mechanisms may contribute to global wave propagation[39,54–58]. In particular, lateral connectivity within the reticular nucleus of thalamus or connectivity linking cortical regions via thalamic intermediaries might play a role coordinating recurrent thalamocortical activity[59–63]. Future studies of the mechanisms of traveling waves in the mammalian brain will need to consider the diverse circuits across the brain that simultaneously reflect their propagation.

What function might these spiral dynamics serve? Oscillatory power in the frequency range that we studied is correlated with behavioral engagement[41], and the momentary phase of spontaneous fluctuations modulates perceptual detectability[5,6]. Therefore, we hypothesize that waves of activity sequentially sweeping across sensory modalities may act to continuously scan these sensory systems, like a radar sweep[1], modulating stimulus detectability in each region. Alternatively, these waves could be involved in guiding plasticity mechanisms[2] to form connections between neighboring somatosensory and motor modalities (e.g., trunk with tail,

hindlimbs with forelimbs, etc) to support behavioral functions that commonly involve sequential motor behaviors across these body parts. Indeed, the spirals we observed have similar properties to those observed during human sleep spindles, suggesting a possible role in memory consolidation[19]. Finally, the presence of these waves in basal ganglia and midbrain, regions traditionally more tightly linked with motor function, raises the question of how these activity patterns avoid interfering with motor control, and future studies may seek to establish with the methods employed here whether these traveling waves are indeed even present at the level of pons, hindbrain, or spinal cord.

Methods

Animals and virus injections

All experimental protocols were conducted according to US National Institutes of Health guidelines for animal research and approved by the Institutional Animal Care and Use Committee at the University of Washington.

The following transgenic mouse lines and viruses were used for this study.

Mouse lines:

Ai210 (B6.Cg-*Igs7*$^{tm210(tetO\text{-}GCaMP7f,CAG\text{-}tTA2)Tasic}$/J, Jax# 037378)

- dual-recombinase responsive (cre/flp-dependent), express tTA2 and jGCaMP7f

Ai195 (B6;129S6-*Igs7*$^{tm195(tetO\text{-}GCaMP7s,CAG\text{-}tTA2)Tasic}$/J, Jax# 034112)

- dual-recombinase responsive (cre/flp-dependent), express tTA2 and jGCaMP7s

Snap25-Cre (B6;129S-*Snap25*$^{tm2.1(cre)Hze}$/J, Jax# 023525)

- knock-in mice with widespread Cre recombinase expression directed throughout the brain

VGlut1-FlpO (B6;129S6-*Slc17a7*$^{em1(flpo)Tasic}$/J, Jax# 034422)

- knock-in mice with optimized FLP recombinase expression directed to VGlut1-expressing cells

VGlut1-Cre (B6;129S-*Slc17a7*$^{tm1.1(cre)Hze}$/J, Jax# 023527)

- knock-in mice with Cre recombinase expression directed to VGlut1-expressing cells

Viruses:

AAV-PHP.eB-GcaMP7s (addgene# 104487-PHPeB): AAV PHP.eB particles produced from pGP-AAV-syn-jGCaMP7s-WPRE (addgene #104487) at titer ≥ 1×10^{13} vg/mL

CAP-B10-soma-jGCaMP8m (gift from Sverre Grødem[64]) : AAV with CNS- and neuronal-specific CAP-B10 serotype produced from pGP-AAV-syn-soma-jGCaMP8m-WPRE (addgene #169257) at titer 3.5 x 10^{12} vg/mL

AAV-PHP.eB-hSyn-Cre (addgene # 105540-PHPeB): AAV PHP.eB particles produced from pENN.AAV.hSyn.HI.eGFP-Cre.WPRE.SV40 (addgene #105540) at titer ≥ 1×10^{13} vg/mL

AAV-PHP.eB-Syn-flpO-WPRE (gift from Tanya Daigle, Allen Institute for Brain Science): AAV PHP.eB particles produced from Syn-FlpO-WPRE at titer 4.1×10^{13} vg/mL

We used four different strategies to express GCaMP7/8 across the brain. (1) Ai210 or Ai195 mice were bred with Snap25-Cre or VGlut1-FlpO, then injected with AAV-PHP.eB-Syn-FlpO or AAV-PHP.eB-hSyn-Cre virus (3-5 μL) retro-orbitally in 4-6 week-old mice for dual cre/FlpO-dependent GCaMP7f or GCaMP7s expression throughout the brain; (2) Ai210 mice were bred with Snap25-Cre positive and VGlut1-FlpO positive mice, to create triple transgenic mice that expressed GCaMP7f in excitatory neurons throughout the brain; (3) Retro-orbital injection of CAP-B10-soma-jGCaMP8m (100 μL) in 4-6 week-old wild type mice; (4) Retro-orbital injection of AAV-PHP.eB-flex-GCaMP7s (40 μL) in 4-6 week-old VGlut1-Cre mice.

Mouse ID	Sex	Age (days)	GCaMP	Genotype	Virus injection	WF sessions	WF+ephys sessions
AB_0004	M	65	jGCaMP7f	Ai210	5μL PHP.eB-flpO	1	0
ZYE_0012	F	50	jGCaMP7f	Ai210	5μL PHP.eB-flpO	1	0
ZYE_0043	F	104	jGCaMP7f	Ai210	5μL PHP.eB-cre	1	1
ZYE_0052	M	86	jGCaMP7f	Ai210	5μL PHP.eB-cre	1	1
ZYE_0053	M	88	jGCaMP7f	Ai210	5μL PHP.eB-cre	0	3
ZYE_0056	F	109	jGCaMP7f	Ai210	5μL PHP.eB-cre	1	0
ZYE_0058	M	167	jGCaMP7f	Ai210	5μL PHP.eB-cre	1	2
ZYE_0059	M	134	jGCaMP7f	Ai210	10μL PHP.eB-cre	1	2
ZYE_0060	M	143	jGCaMP7f	Ai210	10μL PHP.eB-cre	1	2
ZYE_0062	F	149	jGCaMP7f	Ai210	10μL PHP.eB-cre	1	3
LK_0003	M	72	jGCaMP7f	Ai210 triple	/	1	1
ZYE_0048	F	154	jGCaMP7f	Ai210 triple	/	0	2
ZYE_0050	F	148	jGCaMP7f	Ai210 triple	/	0	2
ZYE_0014	F	235	jGCaMP7s	Ai195	3μL PHP.eB-flpO	0	1
ZYE_0038	F	79	jGCaMP7s	Ai195	5μL PHP.eB-cre	0	1
ZYE_0041	F	122	jGCaMP7s	Ai195	5μL PHP.eB-cre	0	4
ZYE_0047	M	74	jGCaMP7s	Ai195	5μL PHP.eB-cre	0	1
LK_0001	M	112	jGCaMP7s	vglut1-cre	40μL PHP.eB- flex-g7s	1	0
ZYE_0066	F	236	jGCaMP8m	wild type	100μL CAP-B10-G8m	0	1
ZYE_0067	F	234	jGCaMP8m	wild type	100μL CAP-B10-G8m	1	1
ZYE_0070	F	102	jGCaMP8m	wild type	100μL CAP-B10-G8m	1	0
ZYE_0071	F	101	jGCaMP8m	wild type	100μL CAP-B10-G8m	1	1
ZYE_0072	M	102	jGCaMP8m	wild type	100μL CAP-B10-G8m	1	0

In total, 23 mice of both sexes with GCaMP expression were used, between 2-8 months old (median at 4 months old) when the first experiment was conducted. 15 mice were used for widefield imaging only experiments, 17 mice (29 sessions) were used for simultaneous widefield and electrophysiological recordings. 9 out of the total 23 mice were used for both experiments. Our findings were consistent across different expression strategies, and therefore we combined these mice in the analysis unless specified.

Surgery

The surgical preparation was similar to that used previously for whole-cortex widefield imaging[65]. Mice were anesthetized under 3-4% isoflurane in an induction chamber first, then maintained at 1-2% isoflurane for the duration of the 1-2 hour procedure. Carprofen (5 mg/kg) was administered subcutaneously and lidocaine (2 mg/kg) was injected under the scalp for postoperative analgesia. The scalp was shaved and further cleaned with hair removal cream before mice were transferred to a separate stereotaxic frame for surgery. Eye ointment (Alcon, Systane) was applied before surgery to prevent drying and body temperature was kept at 37 °C with a far infrared warming pad (Kent Scientific). The skin and periosteum connective tissue was cleared off the dorsal surface of the skull. A layer of cyanoacrylate (Vetbond Tissue Adhesive) was then applied to seal the junction between the exposed skull and cut skin. A 3D-printed plastic recording chamber was implanted on top of the skull with dental cement (C&B Metabond) to provide light isolation during experiments, and a custom-made steel headplate was attached to the skull over the interparietal bone with Metabond for head fixation. To create a clear coating suitable for imaging, we consecutively applied two separate thin layers of fast curing optical adhesive (NOA81, Thorlabs) and cured until solidification with a 365 nm, 3 W output power UV Flashlight (LIGHTFE, UV301D). Carprofen (0.05 mg/ml) was given for 3 days in water after surgery. Mice were allowed to recover in the home cage for at least 5 days before habituation to head fixation.

Widefield imaging and data processing

The widefield imaging setup was custom-built with a macroscope body (sciMedia fluorescent beam splitter DLFLSP2R) fitted with a CMOS camera with 3.45 μm/pixel resolution (Basler ace acA2440-75 m) and a 0.63x objective lens (Leica Planapo 0.63x). Alternating dual light illumination was generated using an OptoLED system (Cairn Research) with blue (470 nm) and violet (405 nm) LEDs to capture GCaMP calcium signal and hemodynamic intrinsic signal at 35 Hz each, respectively. Images were captured at 70 Hz using external triggers synchronized to the light illumination and binned at 3 x 3 pixels to increase signal-to-noise ratio and reduce data size. This results in a final resolution of 17.3 μm/pixel for the collected imaging data. To reduce light artifacts for Neuropixels recordings during imaging, the LED onset and offset were modified to be a 3-ms sine-wave ramp by controlling the analog voltage output from a microcontroller board (Teensy 3.2), resulting in an effective 11-ms exposure time at full intensity for each frame.

For widefield imaging experiments, mice were acclimated to head-fixation for at least two sessions before recording, following recovery from headplate implant surgery. Head-fixed mice were seated on a plastic tube with forepaws on a left-right rotating rubber wheel[66]. Three iPad screens were positioned around the mouse at right angles. A 3D-printed cone was designed to connect the recording chamber with the macroscope objective in order to shield the subject's eyes from the LEDs and prevent light contamination of the imaging signal. Eye position and facial movements were tracked simultaneously with separate infrared cameras (eye position: Navitar Zoom 7000; facial movement: FLIR Chameleon3) with external infrared illumination (CMVision IR30, 850 nm). Cortical visual areas were mapped using white visual sparse noise squares asynchronously on a black background and visual field sign maps (Extended Data Fig.5) were computed as in Peters et al. (2021)[28].

For widefield data analysis, non-neuronal signals arising from changes in blood flow were removed by subtracting the violet-light evoked signals from the blue-light evoked signals with linear regression, which resulted in an effective sampling rate of GCaMP activity at 35 Hz[65,67,68]. In brief, a scaling factor was first fit for each pixel between two signals that were band-pass filtered in the range of 11-13 Hz (heartbeat frequency, with largest haemodynamic effect expected). The haemodynamic-corrected traces were therefore the blue traces in full frequency range subtracted by the scaled violet traces[28,65]. All widefield data were aligned to the Allen CCF[50] with affine transformation using four anatomical landmarks as in Musall et al. (2019)[68], which were the left, center and right points where the anterior cortex meets the olfactory bulbs, and the medial point at the base of retrosplenial cortex. Alignment results were further verified with retinotopic visual field sign maps, with visual fields aligned within the boundaries of the visual CCF coordinates (Extended Data Fig.5).

To store and process the data effectively, we compressed the widefield data (D) into spatial components (U) and temporal components (S*V) with singular value decomposition in the form $D = USV^T$, as previously described[28,41]. We used the top 50 singular vectors, which accounted for 97.3 ± 0.5% (mean ± SEM, 15 mice) of total variance before compression. We divided the widefield signal by the average fluorescence at each pixel, to get $\Delta F/F$ normalized signal.

Simultaneous Neuropixels recording and widefield imaging

Penetration angles and positions of 4-shank Neuropixels 2.0 probes[69] for subcortical recordings were carefully designed to maximize the coverage of sensory modalities in each subcortical region (thalamus, striatum and midbrain) based on the 3D axonal projection maps from the Allen Mouse Brain Connectivity Atlas[25], using the neuropixels trajectory explorer (https://github.com/petersaj/neuropixels_trajectory_explorer) and Pinpoint software[70]. In detail, eight injection experiments with anterograde virus injection sites at VISp [ID: 309003780], RSP [ID: 166054929], SSp-tr [ID: 100141495], SSp-ul [ID: 112229814], SSp-ll [272698650], SSp-m [ID: 157654817], SSp-n [ID: 168163498], SSp-bfd [ID: 127866392] were selected and 3D projection density volumes were downloaded from the Allen Mouse Brain Connectivity Atlas. Intensity-weighted centers of the eight projections within each subcortical region (thalamus, striatum and midbrain) were identified, and a 2D plane was fitted from these center points.

Optimal angles and depths of the 4-shank probe were then selected within the fitted 2D plane, which covered most of the projected center points.

Before moving the 4-shank probes with the angle and depth parameters below, the 2D face of the 4-shank probe was positioned perpendicular to the AP (anterior-posterior) axis of the brain and above the right hemisphere of the brain. All angle and depth parameters were measured for the first shank that was closest to the sagittal suture. For striatal recordings, we used two angle strategies, (1) from the method described above and (2) parameters from Peters et al. 2021[28], where the authors mapped cortical-striatal functional correspondence. AP coordinates were referenced to the bregma position, ML (medial-lateral) coordinates were referenced to the sagittal suture, azimuth angles were counterclockwise rotation around the DV(dorsal-ventral) axis from the dorsal-to-ventral view, elevation angles were clockwise rotation around the AP axis from the posterior-to-anterior view, spin angles were counterclockwise rotation around the probe axis from the probe base-to-tip view.

	AP	ML	Azimuth	Elevation	Spin	Depth	Entry hemisphere	Target hemisphere
Thalamus	2.9 mm	3.5 mm	50°	45°	57°	4.7 mm	Right	Right
Striatum1	2.1 mm	2.9 mm	9°	33°	51°	4.3 mm	Right	Right
Striatum2	0 mm	1 mm	90°	45°	90°	6 mm	Right	Left
Midbrain	3.6 mm	1 mm	107°	45°	0°	3.2 mm	Right	Left

On or before the first day of recording, a 1-2 mm diameter craniotomy was prepared with a dental drill over the target brain area under anesthesia, leaving the dura intact. The craniotomy was protected with transparent dura-gel (Dow Corning 3-4680 Silicone Gel), with a further 3-D printed protective cap sitting on top of the recording chamber. After several hours of recovery, mice were head-fixed in the recording setup. A light shield cone was installed to connect between the recording chamber and the top edges of the ipad screens to block imaging light from the mouse's eyes while achieving maximum probe angle flexibility. We used internal reference configuration for all recordings, with ground and reference connected. In detail, a probe was directly inserted through the dura gel without solution bath and the reference site on the probe tip was used for grounding and referencing. Prior to each insertion, the electrode shanks were coated with CM-DiI (Invitrogen), a red lipophilic dye, for later histological reconstruction of probe tracks.

Histology

To recover electrode tracks, the brain tissue was first extracted after perfusion with 4% formaldehyde under terminal anesthesia, followed by tissue clearance with the iDISCO protocol [71]. Image stacks of the brain sample were acquired with a light-sheet microscope (LaVision Biotec UltraScope II) at 561 nm excitation channel for DiI and 488 nm for autofluorescence. The 3D sample volume was then registered to Allen CCF[50] using open source package 'ara_tools' based on image registration suite Elastix (https://github.com/SainsburyWellcomeCentre/ara_tools). The electrode tracks were manually

traced within the 3D sample volume space using open source package 'lasagna' (https://github.com/SainsburyWellcomeCentre/lasagna).

Power spectrum analysis (Extended Data Fig.1)

To compute the power in the 2-8 Hz frequency band across the cortex efficiently, we computed the power spectrum on the temporal components of the data (S*V) after singular value decomposition, and transformed the power spectrum back to the 2-dimensional space by multiplying the spatial components (U)[41]. Power spectrum was performed using multitaper fourier transform[72] and averaged across multiple 2-second epochs of data. Power spectrum was normalized by peak power in each mouse first, before averaged across mice. Power across 2-8 Hz were then summated to construct a 2-8 Hz "power map" across the cortical pixels (Extended Data Fig.1). We also used a fast Fourier transform approach to construct the 2-8 Hz "power map" and achieved the same results (data not shown).

Spiral detection and quantification

Spiral detection algorithm (Fig.1, Extended Data Fig.1, Extended Data Fig.2)

To capture the dynamics of the widefield time series data, we first took the first-order derivative of the calcium traces, approximating a deconvolution to better match underlying firing rates[65], and then filtered the traces with a second-order Butterworth bandpass filter at 2-8 Hz with zero phase distortion. To extract the spatial distribution of the oscillation phase angle over time, the Hilbert transform is applied after filtering to each pixel independently. For visualization, the phase information for all pixels was plotted together to construct phase maps over time (Fig.1a,b, Extended Data Fig1).

To automatically detect spirals (Extended Data Fig.2), we took advantage of the fact that phase angles along the spiral circle for any given radius cumulatively increase by 2π. We designed a three-step algorithm with a coarse-to-fine approach to identify spiral centers and radii. Step 1: Coarse grid search for spirals. Each frame is zero padded with 120 extra pixels (2 mm) on each of the four edges first to effectively detect spirals near the edge or with large radii. Spirals were first identified on a coarse grid (10 x 10 pixels, 173 x173 μm spacing). Since the phase angle distribution within a spiral is noisy at times, we defined two broad criteria for spiral detection: (1) angular differences of 10 evenly sampled points along the spiral circle cumulatively added up to near $\pm 2\pi$ ($2\pi \pm 0.32\pi$), with opposite signs representing clockwise and counterclockwise spiral directions; (2) at least one out of the 10 points sampled lies in each of the 4 quadrants within 0 to 2π range. At each search grid, 3 small circles (radii at 10,15, 20 pixels, which are 173, 260, 346 μm) were sampled independently. If at least 2 out of 3 sampled circles passed the two criteria above, then the grid coordinate was considered a candidate spiral position. Step 2: Clustering nearby candidate spiral centers. A robust spiral was often detected at multiple nearby candidate grid points. Spiral centers separated by a Euclidean distance less than 15 pixels (260

μm) were grouped together, and the mean coordinate of the group was taken as the intermediate candidate spiral center. Step 3: Refined spiral search and radius determination. The final positions of spirals were refined with the same algorithm from step 1 and 2 within a 20 x 20 pixels ROI at full resolution based on the intermediate candidate spiral coordinates from step 2 through a pixel-by-pixel search. The final radius was tested from 10 to 100 pixel values at 10 pixel steps (from 17.3 μm to 173 μm, at 17.3 μm steps), and the maximum radius was identified as the largest radius for which the two criteria in Step 1 were satisfied.

Phase randomization control for spiral occurrence (Extended Data Fig.3)

Spirals can randomly occur within spatially and temporally smooth dynamics. To ensure that the spirals we observed were not by chance, we constructed surrogate data using a Fourier-based phase randomization, which preserved both the spatial and temporal correlations of the raw data[21,73]. We performed the fast Fourier transform on the 3D raw data (x, y, t), randomized the phase values of the Fourier components by shuffling the index of the 3D phase matrix, and then reconstructed surrogate data with the inverse Fourier transform. To avoid including areas outside of the brain in the anterior space for the Fourier transform, we drew a rectangle in the posterior cortex and used only this area for both raw data and surrogate data comparison. We then applied the spiral detection algorithm to the raw data and surrogate data within the rectangle region, and compared distributions of detected spirals (Extended Data Fig.3). Peak spiral density for spirals with radius greater than or equal to 0.69 mm within the somatosensory cortex (SSp) were significantly higher in the real data than in the surrogate data across 15 mice tested (Extended Data Fig.3). Therefore, we only included spirals that had radius greater than or equal to 0.69 mm for further analysis.

Spiral sequences and permutation control (Fig. 1)

To group traveling spirals into spatiotemporally connected spiral sequences, we classified spirals that were less than 30 pixels (0.5 mm) apart in Euclidean distance in neighboring frames to be in the same sequence group (Fig.1d). To determine whether the spiral sequences we observed could arise from chance with the same overall rate of spiral occurrence, we permuted the frame identity for all included spirals (those with radius greater than or equal to 0.69 mm) within a session 1000 times and recomputed the sequence grouping. Proportions of spirals that belonged to a sequence with duration lasting for more than one frame (29 ms) were consistently and significantly lower in the permutations compared to our observed data ($p < 1\text{x}10^{-7}$,unbalanced two-way anova; Fig.1d), while the proportion of single-frame spirals in the permuted distribution was significantly higher than in observed data ($p < 1\text{x}10^{-7}$, student's t-test; Fig.1d). We therefore excluded single-frame spirals from further analysis. Nevertheless, single-frame spirals (29 ms) were also spatially concentrated within the SSp center (Extended Data Fig.6).

Spirals in the cortical LFP activity (Extended Data Fig.4)

To capture spiral waves in the cortical LFP activity without GCaMP sensors, we inserted a 4-shank Neuropixels probe with 0.7-mm span of active sites on each shank in wild type C57BL/6 mice at a shallow angle in the middle of SSp (Extended Data Fig.4). The shallow angle helped us record as many SSp regions as possible in a single recording, since a steep probe angle usually captures neural activity in a single region across layers. LFP was downsampled to 35 Hz after applying a low pass filter at 17 Hz. To investigate traveling waves within the same frequency range as the widefield data in GCaMP expressing mice, we then applied a second-order Butterworth bandpass filter at 2-8 Hz and the Hilbert transform for each individual site. All sites were then rearranged as a 8x48 site matrix based on probe site location, and LFP activity map and phase maps over time were plotted (Extended Data Fig.4).

Spiral center density estimation (Fig.1, Extended Data Fig.5, Extended Data Fig.6)

To estimate the spatial density of spiral centers in cortex, we drew a local square (0.4*0.4 mm^2) around each unique spiral and counted total spiral centers within the square. All spirals (with radius greater than or equal to 0.69 mm) that were within a spiral sequence (>= 2 frames) were included for the spiral center density plot. Given total frame numbers within a session and the sampling frequency of 35 Hz, we then converted these counts to density rates with units of spirals/(mm^2*s). For the summary spiral density plot (Fig.1e), all 15 sessions were concatenated for spiral density estimation.

Spiral symmetry quantification (Fig.2, Extended Data Fig.7)

Three peaks in the spiral center density plot were observed on each hemispheres, centered on SSp, MOp and MOs respectively (Fig.1, Extended Data Fig.7).To determine whether spirals are symmetrical and therefore are traveling in opposite directions in neighboring structures, we grouped all detected spirals into 6 regions for quantification: SSp, MOp and MOs regions in the left and right hemisphere. The borders between regions were based on Allen CCF[50] after alignment in Methods “Widefield imaging and data processing”. We compared spiral directions between MOp and SSp within each hemisphere (left MOp-SSp, right MOp-SSp), MOp and MOs within each hemisphere (left MOp-MOs, right MOp-MOs), and between each of the three regions across hemispheres (SSp left-right, MOp left-right, MOs left-right). When a pair of spirals were detected simultaneously in a single frame in both neighboring regions, the directions of the spirals were compared. When the two neighboring spirals were traveling in opposite directions, they were considered to be matched, in the sense that our hypothesis based on the mirrored topographic organization of these regions[26] predicted mirrored dynamics.

Synchrony and spirality index (Extended Data Fig.8)

To quantify traveling waves across all frames, we designed a synchrony index and a spirality index (Extended Data Fig.8). Synchrony index (Rsync) is the mean resultant vector length of all phase angles in a frame (1-circular variance):

$$Rsync = \frac{\left|\sum_{x=1}^{m}\sum_{y=1}^{n} e^{i\cdot\alpha_{x,y}}\right|}{m \times n}$$

where $\alpha_{x,y}$ is the phase angle of the [x, y] -th pixel within a frame with frame size [m, n]. Synchrony index (Rsync) is bound between 0 and 1. Synchrony index close to 0 indicates all phase angles are random and Synchrony index close to 1 indicates all phase angles are uniform.

However, the synchrony index does not differentiate spiral patterns from randomness. The synchrony index for spiral-like patterns is also close to 0, since all phases with opposing directions are represented in a spiral. Therefore we designed a spirality index (Rspiral), to quantify how close the phase map (A) from a single hemisphere of size [m, n/2] from a sampled frame with size [m, n], matched to a perfect spiral template (B) of the same size ([m, n/2], Extended Data Fig.8). Angles (β) within the spiral template (B) were constructed with a four-quadrant inverse tangent function of the position matrix [u_x, v_y], which were bound in the closed interval [-π, π]:

$$\beta_{x,y} = atan2(v_y, u_x),\ where\ u_x = -\frac{m}{2}:\frac{m}{2},\ v_y = -\frac{n}{4}:\frac{n}{4}$$

Spirality index (Rspiral) is the mean resultant vector (1-circular variance) of the angular difference map (θ):

$$Rspiral = \frac{\left|\sum_{x=1}^{m}\sum_{y=1}^{n/2} e^{i\cdot\theta_{x,y}}\right|}{m \times n/2},$$

$$\theta_{x,y} = \alpha_{x,y} - \beta_{x,y},$$

where θ is the angular difference between phase angles (α) in a sampled half-hemisphere frame (A) with [m, n/2] size and a spiral phase template (β) with a perfect spiral (B) of the same size. 0 indicates no spiral-like features in the frame, while 1 indicates a spiral-like frame.

Sum index (S) is defined as:

$$S = \sqrt{Rsync^2 + Rspiral^2},$$

which is also bounded between 0 and 1, as frames with high synchrony index have low spirality index and vice versa (Extended Data Fig.8).

We thereafter quantified the relationship between (1) synchrony index (or spirality index) and (2) mean 2-8 Hz amplitude (or facial motion energy), by averaging the synchrony index (or spirality index) for frames within each mean 2-8 Hz amplitude (or facial motion energy) bin. Mean 2-8 Hz amplitude for each frame was calculated as the mean 2-8 Hz amplitude across all pixels within the widefield cortex boundary. The amplitude of 2-8 Hz oscillation for each pixel was the complex magnitude of the analytic signal from the Hilbert transform after second-order Butterworth bandpass filter at 2-8 Hz for each pixel trace. The facial motion energy for each frame was calculated as the cross-pixel sum of the absolute difference between consecutive frames.

Spiral speed (Extended Data Fig.9)

We calculated optical flow from sequential pairs of phase-map frames with the Horn-Schunck method [74] to illustrate directions of wave travel (Fig.1c). To quantify spiral wave speed accurately (Extended Data Fig.9), we sampled 12 evenly spaced points on circles of varying distance from spiral center within each detected spiral. We used all spirals within a 1.7x3.4mm square centered on SSp in the right hemisphere across all mice (Fig.1f, g, Extended Data Fig.9). Angular speed (ω, rad/s) for any point within the spiral was calculated with the following equation:

$$\omega = angle(e^{i\cdot(\theta 1-\theta 2)}) \times f ,$$

where $\theta 1$ is the phase angle for the sampled point of current frame, $\theta 2$ is the phase angle for the sampled point of the next frame, f is the sampling frequency (35 Hz). Angular difference is wrapped in the interval [-π, π] with Euler's formula and *angle* function in matlab.

We then calculate linear speed (v):

$$v = r \times \omega,$$

where r is the distance of the sampled point to the spiral center, ω is the angular speed for the sample point.

Single neuron axonal arbor analysis (Fig. 2)

To investigate the morphological basis of spiral waves in the cortex, we used the Single Neuron Reconstruction Dataset[44], in which 1,741 neurons from various brain regions were sparsely labeled and reconstructed after whole-brain imaging. Out of 1,741 neurons throughout the entire brain, 435 neurons were labeled within the sensory cortex. These areas include visual cortex (VIS), auditory cortex (AUD), retrosplenial cortex (RSP), primary somatosensory cortex (SSp) and secondary somatosensory cortex (SSs). To reveal the local axon architecture within the sensory cortex, we excluded long-range axon projections, i.e. projections to the subcortical areas, to the contralateral hemispheres, and to motor areas of cortex. For SSs and AUD, where ipsilateral long-range projections were prevalent, only axons restricted to the local regions (SSs and AUD only) were analyzed. The singular value decomposition was computed for each neuron's 2D point cloud (in the AP-ML plane) of axon terminals (ending points of axon branches). The first singular vector was taken as the dominant direction of the axonal arbor. A "polarity index" was computed to capture the elongation of the axonal arbor:

$$P = \frac{s1}{s2} - 1,$$

where P is the polarity index, s_1 is the first singular value, and s_2 is the second singular value. A polarity index closer to 0 indicates symmetrical distribution of axon terminals on the first two major axes, and larger values indicate a dominant distribution of axon terminals on the first major axis.

Axon-to-SSp-center angle (θ) is calculated as the angle between (1) the axonal first singular vector (s1) and (2) the vector from the SSp center to cell soma. The permuted distribution is generated by scrambling the soma position of each neuron 100 times while preserving the direction of the singular vector, and re-calculating the SSp-center bias.

To compare axon orientations to spirals in the mesoscale activity, we computed a mean spiral flow field by averaging the optical flow across all spirals with a large radius around the SSp center that were counterclockwise traveling in one hemisphere in all 15 mice used. We then sampled flow vectors within the flow field at the soma positions of all 435 sensory neurons used in the axon vector map (u), forming a paired flow vector map (v). We then designed an axon-flow field vector matching index, which is the sum of absolute values of the dot product of all axon vectors (u) and flow field vectors (v) at the same soma location.

$$Index = \sum_{i=1}^{n} \left| dot(u_i, v_i) \right| .$$

If angles between two vectors at the same soma location are ±90 degrees, then the dot product is zero; if they are matching either at 0 or 180 degrees, the dot product is maximized. Axon vector length is the polarity index (P) of the neuron. The null hypothesis that axon polarity is unrelated to activity flow vectors was tested by permuting the flow vectors, i.e. assigning each of the 435 spatial coordinates to have a flow vector randomly drawn without replacement from the set of all 435 flow vectors in the original map. The null distribution was generated by permuting the flow vector map 1000 times and recalculating the matching index.

Coupled oscillators with circular connectivity bias (Extended Data Fig.10)

In order to capture spiral waves mathematically, we built a minimal model of spatially-coupled phase oscillators which could be naturally extended to include circular connectivity bias [75,76]. We begin by generating a uniformly random point set in 2D space (Extended Data Fig.10), with decaying effective coupling weight (W_{ij}) for each pair of node i and node j proportional to their Euclidean distance d_{ij}, mimicking cortical connectivity[77,78].

$$W_{ij} = W_o e^{-d_{ij}/L},$$

where d_{ij} is the Euclidean distance between node i and node j in the random point set, L is the effective length scale of coupling, and W_o is the scale of the coupling matrix. Consistent with previous results[78,79], traveling waves naturally emerged when L was small (e.g. the coupling is local) and W_o was sufficiently large to pull oscillators into agreement (Extended Data Fig.10). We call this model an isotropic model, in comparison to the circular bias model later.

Having established the presence of traveling waves, we sought to characterize the presence of spiral waves in this baseline model for spatially coupled oscillators (Extended Data Fig.10). As a complementary tool to study the presence of spiral waves, we leveraged a population scale

metric related to synchronization to look for the presence or absence of spirality (Sp), which is same to the definition of Spirality index (Rspiral) as described in Methods section "Synchrony and spirality index" (Extended Data Fig.8):

$$Sp(t) = 1/N \sum_{j=1}^{N} e^{i(\phi_j(t) - atan2(y_j/x_j))},$$

where $Sp(t)$ is the spirality at time t, [x_j, y_j] is the position index for the j-th node in the 2D random point set, $\phi_j(t)$ is the phase value of the j-th node at time t, N is the total number of nodes in the 2D random point set.

Spirality (Sp) measures how close the current configuration is to the perfect spiral configuration centered at the center of the field of view on a scale of 0 to 1, with 1 only being achieved when the full field is a spiral centered in the field of view. Equipped with this tool, we sought to characterize spiral waves in our baseline model. Across 1000 simulations (robust against 10 random seeds), we found that spiral waves were more likely near the transition between a desynchronized regime and a synchronized regime. In the crossover vicinity (reflected by noise and scale of coupling critical line separating these two regimes), we observed a dramatic uptick in the spirality of these fields (Extended Data Fig.10). We interpret this result as consistent with the proliferation of defects in a continuous spin-system as it undergoes a BKT transition [80,81]. In the desynchronized regime, there were many defects (including spiral waves) with very short lifetimes as they bounced around and annihilated each other under noisy driving. In the synchronized regime, the dominant defect was the spiral wave because they were topologically protected against continuous deformations leaving them only to find an opposite spiral to annihilate or leave/enter through the boundary of the domain.

To construct a model with circular connectivity bias (Extended Data Fig.10), we defined a nondimensional parameter (σ): $\sigma = \frac{W_{Circular}}{W_{Radial}}$, where $W_{Circular}$ is the circular connectivity strength and W_{Radial} is the radial connectivity strength. W_{Radial} points to the direction of the radial vector connecting the center of the neuron pair under study to the center of the domain (2D random point space), while $W_{Circular}$ points to the direction of tangential edge that connect around a ring, which is orthogonal to W_{Radial}. The coupling weight (W'_{ij}) can therefore be turnably adjusted to have a strong circular bias with a higher σ value through:

$$W'_{ij} = W_{ij} \times (cos^2(\theta) + \sigma sin^2(\theta)),$$

where θ is the angle between (1) the vector formed by the node pair and (2) the radial direction for the center of the node pair to the center of the domain, W_{ij} is the coupling weight defined by the Euclidean distance between node i and j in the isotropic model. The adjusted coupling weights are thereafter normalized by the mean of all weights.

When sigma is greater than 1, there is an azimuthal bias; if equal to 1, the connectivity is isotropic; and when less than 1, the connectivity has a radial bias. Combining this with an exploration of the phase space, we find that azimuthal connectivity bias $\sigma = 50$, resulted in

significant stabilization of spirals even against larger mean connectivity strength, while spirals were rapidly ejected from the domain in the baseline model at the same mean connectivity strength, resulting in phase synchronization at all nodes (Extended Data Fig.10).

Linear regression within cortex (Fig.3, Extended Data Fig.11)

Reduced rank regression was applied to predict the posterior sensory cortical activity from the anterior motor cortex, and to predict the right hemisphere from the left hemisphere. Reduced rank regression has the advantage of finding the subspace of regressor activity that is maximally predictive of the target activity, thus acting as both a regularization and a characterization of dimensionality[82]. To divide the anterior/posterior cortex as regressor and target, widefield data (X*Y*t) was first registered to allen brain atlas CCF coordinates[50], and divided into anterior cortical data and posterior cortical data along the border of SSp and MOp respecting the connectivity reciprocity [26] and spiral symmetry we observed. To divide the left/right cortex, the midline was chosen as the dividing line after registration. The first 20-minutes of the widefield data in each session was used as training data, and a 10-minute data section following the training data was used as testing data for cross validation. To account for data collinearity, we applied singular value decomposition ($D = USV^T$) on the regressor data and used the top 50 temporal components (S*V) as the regressor in the regression model, which accounted for 97.3 ± 0.5% (mean ± SEM, 15 mice) of total variance before compression, as previously stated in Method “Widefield imaging and data processing” section. The target data was kept in the original data space (pixels*t). Prediction accuracy was calculated using Coefficient of determination (R^2) on the testing dataset:

$$R^2 = 1 - \frac{SS_{res}}{SS_{tot}}, \; where \; SS_{res} = \sum_i (y_i - \hat{y}_i)^2, \; SS_{tot} = \sum_i (y_i - \bar{y})^2$$

where SS_{res} is the residual sum of squares, SS_{tot} is the total sum of squares, y_i is the i-th value in the observed data, $\hat{y}_i$ is the predicted data, $\bar{y}$ is the mean of the observed data.

To visualize the regression kernel representation in the cortex space, the regression kernel was first transformed back to the pixel space. Kernel maps for example pixels were presented as different color plots overlaid with transparency scaled by kernel weights (Fig.3d-g,h,j, Extended Data Fig.11). Example regressor pixels in Fig.3d-g were chosen as the pixel with maximum value in the weight matrix.

Bulk axon projection map and matching index (Fig.3)

To visualize the long range axon projection maps from sensory cortex to the contralateral hemisphere, or to the motor cortex, we selected eight viral tracer injection experiments targeting eight different sensory modalities within the sensory cortex from the Allen Mouse Brain Connectivity Atlas[25]. The same session IDs were used to identify Neuropixels targeting angles and positions in the subcortical areas in Methods “Simultaneous Neuropixels recording and widefield imaging” section. To combine axon projection maps together, intensity values for injection sites in the sensory cortex were masked first and then normalized across sessions to

account for intensity differences between injection site and target axon region, as well as differences across sessions respectively.

To quantify whether the activity kernel patterns and axon projection patterns matched, we designed a pattern matching index (PIndex) which is the sum of matrix dot product between activity kernel and axon projection map of the same size across all 8 different sampled sensory areas:

$$PIndex = \sum_{i=1}^{n} dot(A_i, B_i),$$

where A_i is the activity kernel for one of the n (n = 8) sampled sensory areas, B_i is the axon projection map for one of the 8 sampled sensory areas.

We used a single common axon projection session for each of 8 sensory areas to compute the matching index, together with mean activity maps across 15 mice. Small variations were observed between the activity map and the axon projection map due to variations of brain registration for each mouse, as well as the slight difference of sampling points for activity map and projection maps. However, the general patterns of both maps matched well for left-to-right hemispheres (Fig.3h,i) and motor-to-sensory cortex (Fig.j,k), compared to permutation. Permutation was performed by randomizing the identity of the 8 axon projection maps 1000 times.

Spiral prediction from subcortical spiking activity (Fig.4, Extended Data Fig.12)

Kilosort2[83] was used for spike sorting of the electrophysiology data from 4-shank Neuropixels recordings. Single neurons were manually curated through Phy (https://github.com/cortex-lab/phy), with violation of refractory period in spike time auto-correlogram as the main criteria for selection. Spikes of each single neuron were then binned at the widefield imaging sampling frequency (35Hz) to match the time series of the imaging data.

To predict cortical widefield data from subcortical spike data (Fig.4b,c), time series of spiking neurons were used to predict the derivative of top 50 temporal components of the cortical widefield data. To predict the full length of the widefield data from subcortical spiking activity, we used 2-fold cross-validation. In detail, we first split the data into 10 equal-length epochs. Then we used the concatenated 5 odd-numbered epochs to predict the held-out even epochs, and vice versa. The mean variance explained map was calculated as the average of the two predictions. To account for the latency between cortical widefield data and spike data, time-shifted spiking series from -17 to 17 samples (-0.5 to 0.5 s at ~0.03 s time steps) were also concatenated into the regressor matrix. For quality control purposes, only sessions with mean variance explained exceeding 10% were included for further analysis (29/46 sessions).

To compare spirals in the raw and predicted cortical activity (Fig.4d,e,g), we took the derivative of the temporal components of the raw and predicted data, and reconstructed the data in pixel space (X*Y*t) after a bandpass 2-8 Hz filter. We then detected spirals in both raw and predicted cortical data by applying the automated spiral detection algorithm. Spirals in the raw cortical activity with significant radius (greater than or equal to 0.69 mm) and duration (longer than 29 ms), were considered for spiral direction comparison. Selection criteria were not applied to the predicted spirals, to maximize the numbers of corresponding spirals included in the subsequent matching test. For each spiral in the raw cortical activity, if only one corresponding spiral was found within 1 mm radius in the predicted cortical activity in the same frame, then the pair of spirals was considered as a candidate pair. We then compared the spiral directions (clockwise or counterclockwise) for all pairs of candidate spirals, and computed the spiral matching probability as the ratio of matching spiral pairs out of all candidate spiral pairs. Here, 'matching' means that the raw and predicted spirals share the same direction. To test the null hypothesis that neurons in the subcortical area did not share spatiotemporal relationships with the cortical data, and that matching spirals therefore only arose by chance or by shared temporal (not spatial) relationships, we first predicted cortical activity by using subcortical spiking activity with permuted neuron identities during linear regression prediction without retraining the model, and then applied the same automated spiral detection algorithm for the permuted prediction. We computed the spiral matching probability between the raw and permuted prediction as control.

Traveling wave quantification with optical flow (Fig.4, Extended Data Fig.12, Extended Data Fig.13)

To quantify traveling waves within the cortical widefield activity (Fig.4, Extended Data Fig.12), we estimated instantaneous velocity for each pixel in the cortex using phase information from nearby two frames. In detail, the derivative of the widefield data was first bandpass Butterworth filtered within 2-8 Hz, and the Hilbert transform was then applied to each pixel independently to extract phase information at each time point to construct the phase maps. We then applied the Horn-Schunck method [74] to extract optical flow from the phase maps of adjacent frames, which used an optimization approach to estimate instantaneous velocity with a global constraint of smoothness.

To compare phase maps and traveling waves of the raw and predicted cortical activity from subcortical spiking activity (Fig.4h,i, Extended Data Fig.12, Extended Data Fig.13), we designed frame-to-frame " phase matching index" and "traveling wave matching index". First, the angular differences of the phase values or the optical flow vectors between raw and predicted data were calculated for pixels in each frame with frame size [m,n]. Phase or traveling wave matching index (M) is the mean resultant vector length of the angular difference map in a frame (1-circular variance):

$$M = \frac{\left| \sum_{x=1}^{m} \sum_{y=1}^{n} e^{i \cdot \theta_{x,y}} \right|}{m \times n},$$

where $\theta_{x,y}$ is the phase angular differences of the [x, y]-th pixel between a raw and predicted frame. MIndex is bound between 0 and 1. M close to 0 indicates all angular difference values

are randomly distributed and not matching, while M close to 1 indicates all angular difference values are uniformly distributed and matching.

To summarize the observation that phase or traveling wave matching index increased as mean 2-8 Hz amplitude in the cortex increased within a session (Fig.4h,i, Extended Data Fig.13), we binned frames based on the mean 2-8 Hz amplitude and calculated the mean matching index within each amplitude bin. Only pixels with cross-validated variance explained greater than 0.1 were included in the final phase or wave matching index calculation. To construct the null distribution, we employed the same strategy as described above for spiral matching, by randomizing the subcortical neuron identities in the testing dataset for regression prediction 20 times, without re-training the model. Phase and wave matching index were then calculated between the raw phase (or traveling waves) and permuted predictions, as control distributions.

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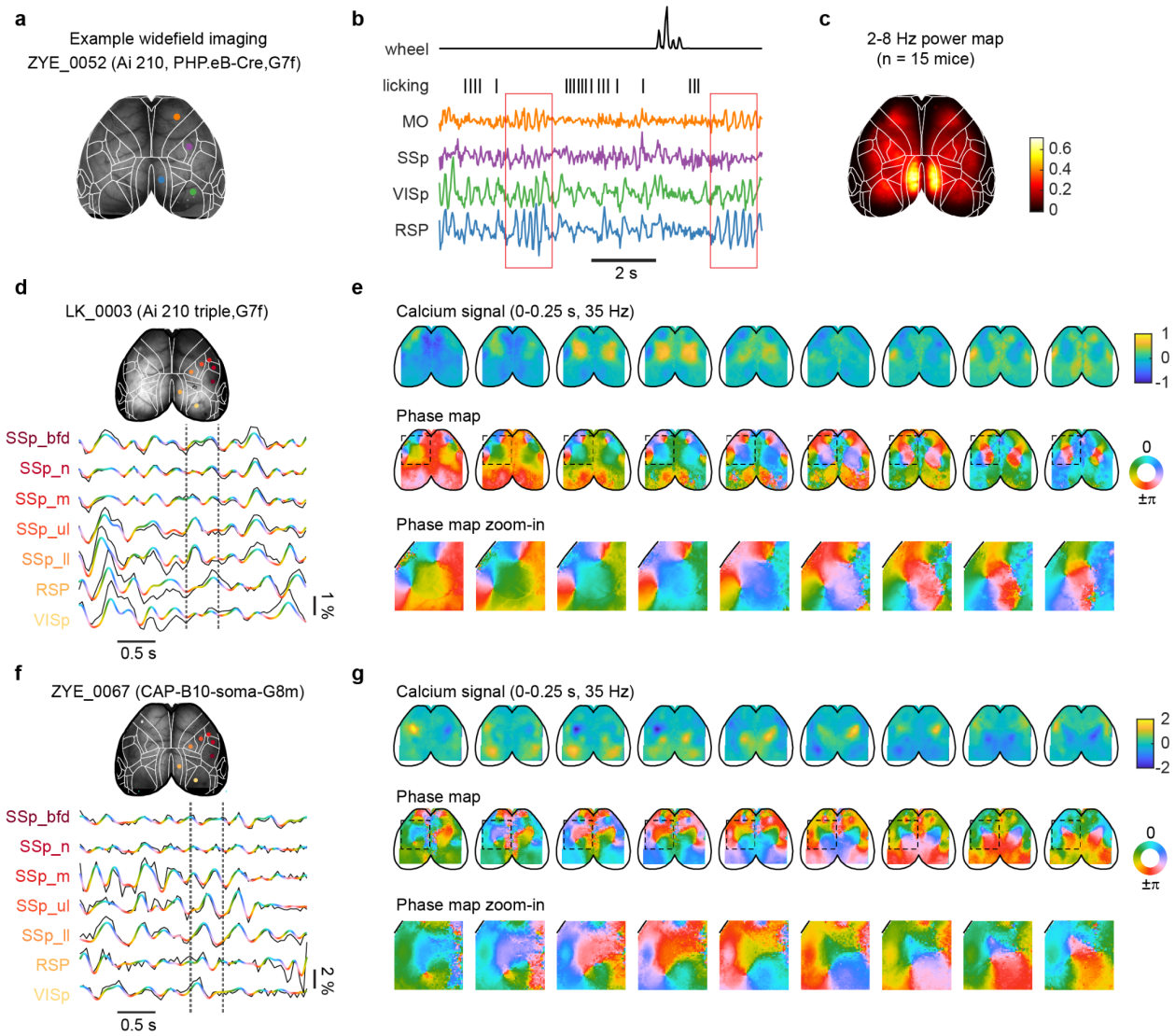
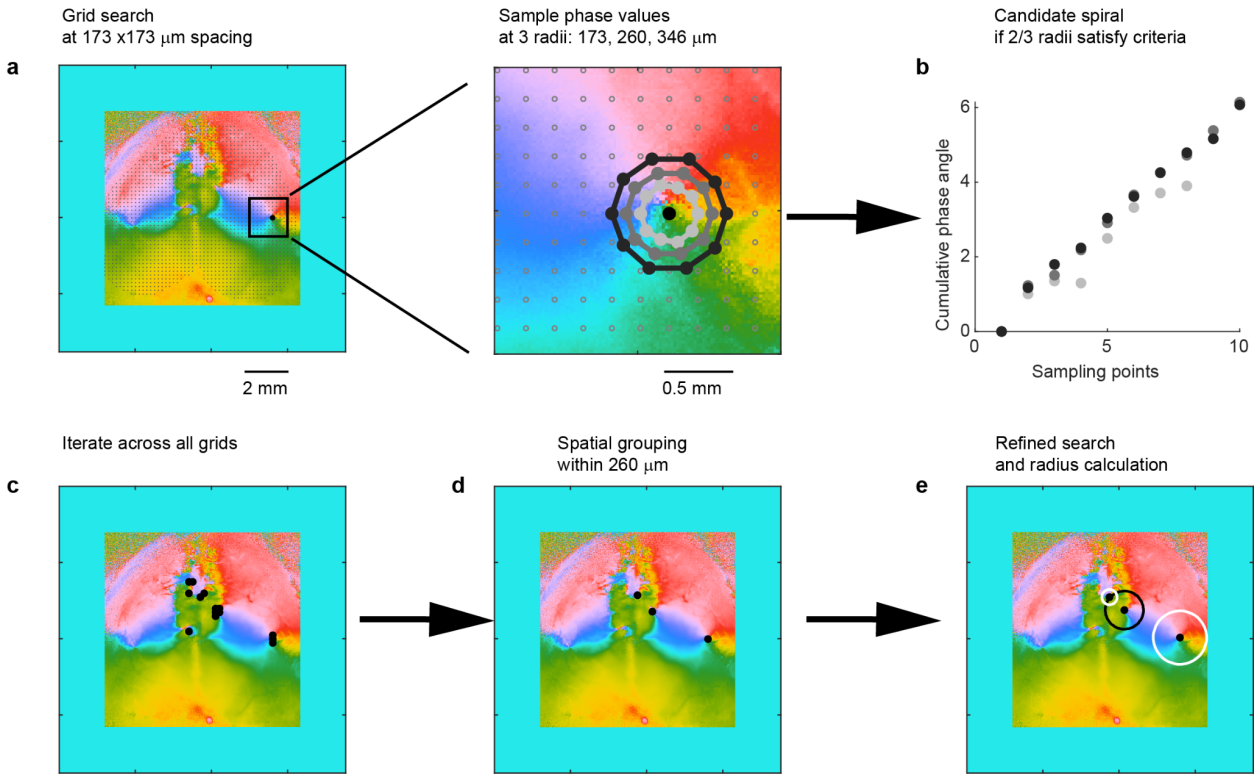
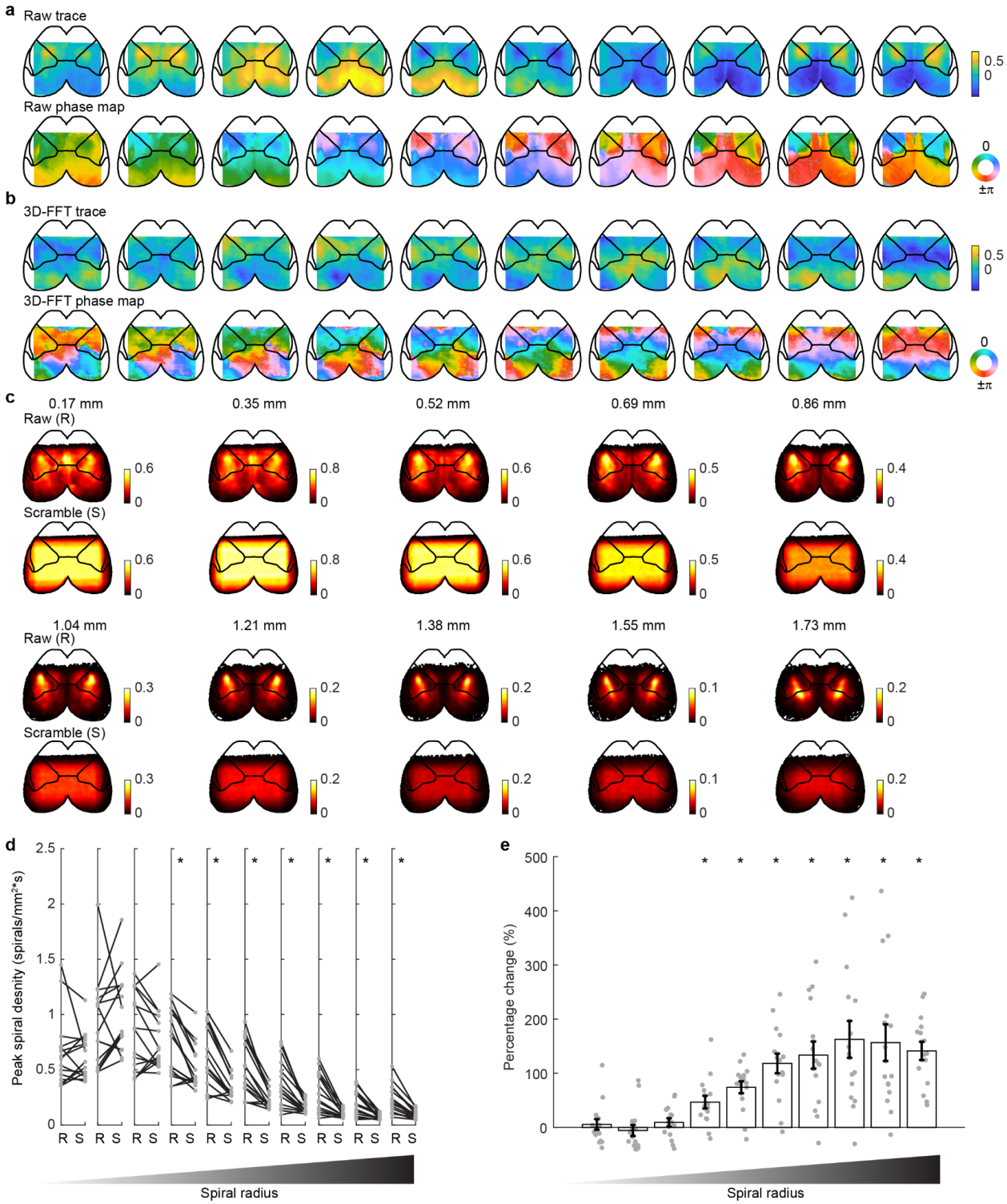
Supplementary Figures



Extended Data Fig.1 | 2-8 Hz power is globally distributed within the cortex and spirals pervades the mouse cortex with different transgenic strategies. a, Example dorsal surface of the mouse cortex for widefield imaging in a mouse with GCaMP7f expression (ZYE_0052, Ai210 mouse injected with PHP.eB-Cre virus). The brain surface was registered to the CCF atlas[50], and outlines of cortical regions superimposed. **b**, Example calcium traces from an awake, behaving mouse, with pixel locations highlighted in **a**. Randomly timed rewards were delivered, provoking licking and ensuring wakefulness. Two epochs of neural activity with strong 2-8 Hz oscillations between lick periods are highlighted in red boxes. **c**, Spatial distribution of averaged power spectrum in the 2-8 Hz frequency range in 15 mice, with highest power in the retrosplenial cortex and with significant power across cortex. **d**, Example calcium traces in a mouse with GCaMP7f expression (LK_0003, Ai210 triple transgenic mouse). Raw traces (black) are overlaid with 2-8 Hz filtered traces color coded by phase values after the Hilbert transform. **e**, 9 example consecutive frames (0.25 s) of calcium signal maps (top), phase maps (middle) and spiral zoom-in (bottom) within the dashed line in **d**. **f**,**g**, Same as in **d**,**e**, but for a mouse with soma-targeted GCaMP8m expression (ZYE_0067, wild-type mouse injected with CAP-B10-soma-GCaMP8m).

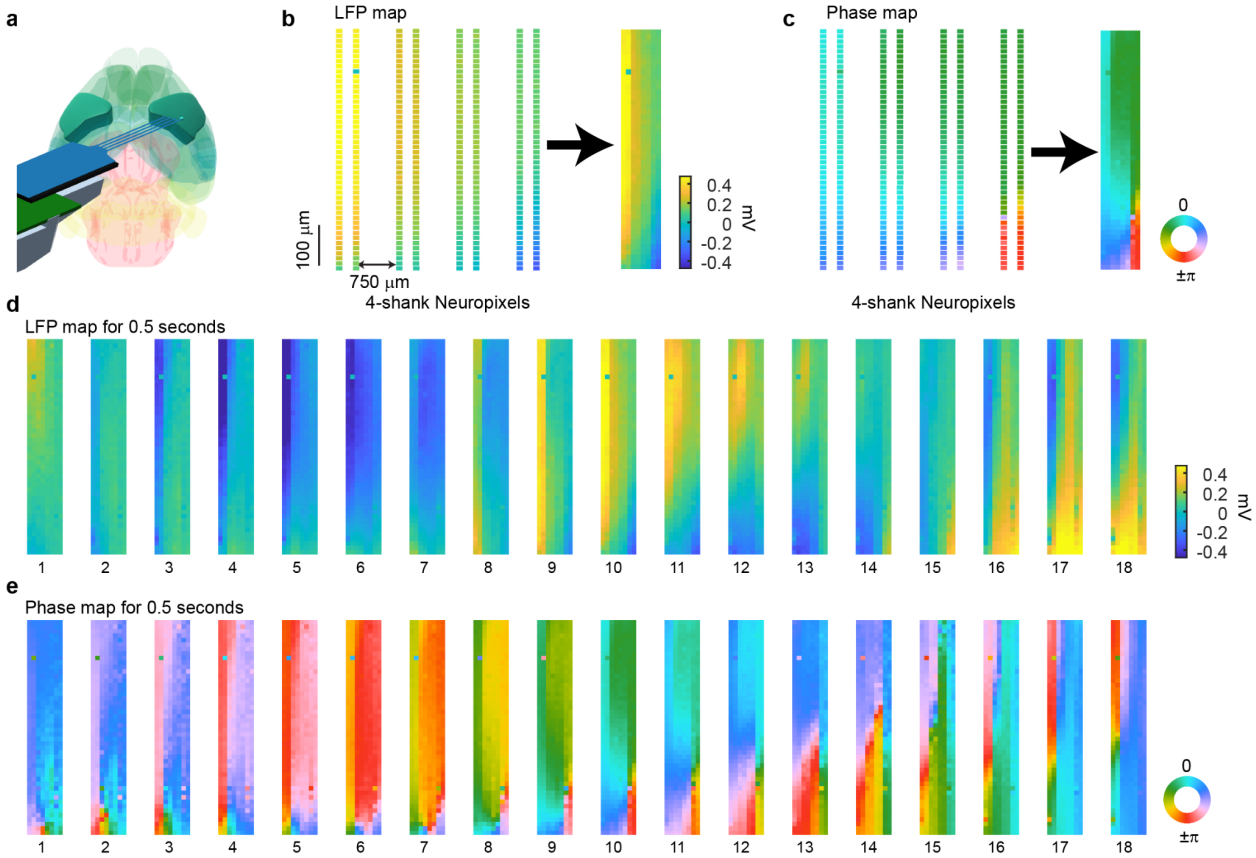


Extended Data Fig.2| Spiral detection algorithm. A three-step process was used to identify spirals, first using a coarse grid search to identify candidate spiral centers, second by clustering nearby candidates, and third by performing a fine search to precisely identify the spiral center and radius. **a**, Phase map frames were zero-padded at the edges and search grids (10x10 pixels, 173 x 173 μm spacing) were drawn on top of the frame within the brain ROI. At each search grid, 3 small circles were drawn (radius at 10, 15, 20 pixels, which are 173, 260, 346 μm). Within each circle, 10 phase values at equal angular spacing (from 0 to 9/5*π at π/5 steps) were sampled. **b**, If the absolute cumulative angular difference from the first to the last sample was close to 2π (2*π ± 0.32π) and there was at least one sample at each of the 4 quadrants of the circular phase angles, then that circle was spiral-like. A grid point was a candidate spiral center if at least 2 out of 3 sampled circles were spiral-like. **c**, Candidate spiral search was iterated across all grids. Black dots represent all candidate spiral centers that were detected in a single frame. **d**, A robust spiral was often detected at multiple nearby grids. Spiral centers that were located within 15 pixels (260 μm) Euclidean distance were grouped together, and the mean location of the spirals within a single cluster was taken as the starting point for a final coarse-to-fine search in the next step. **e**, The precise location of the spiral was then determined by a final refined search approach. A 21x21 pixel ROI centering the spiral candidate (grid points) was extracted, step **a**-**c** is repeated pixel-by-pixel, and final spiral center location is determined. Spiral radius was then determined by the maximum radius that satisfied criteria in **b**. If the cumulative angular difference from the first to the last sample is positive, then the spiral is counterclockwise traveling (white circle); otherwise, clockwise traveling (black circle). Spirals with radius less than 0.69 mm (the smallest spiral in **e** as an example) were excluded in the final analysis, as their distribution did not pass permutation tests and were more likely to be noise (Extended Data Fig.3).



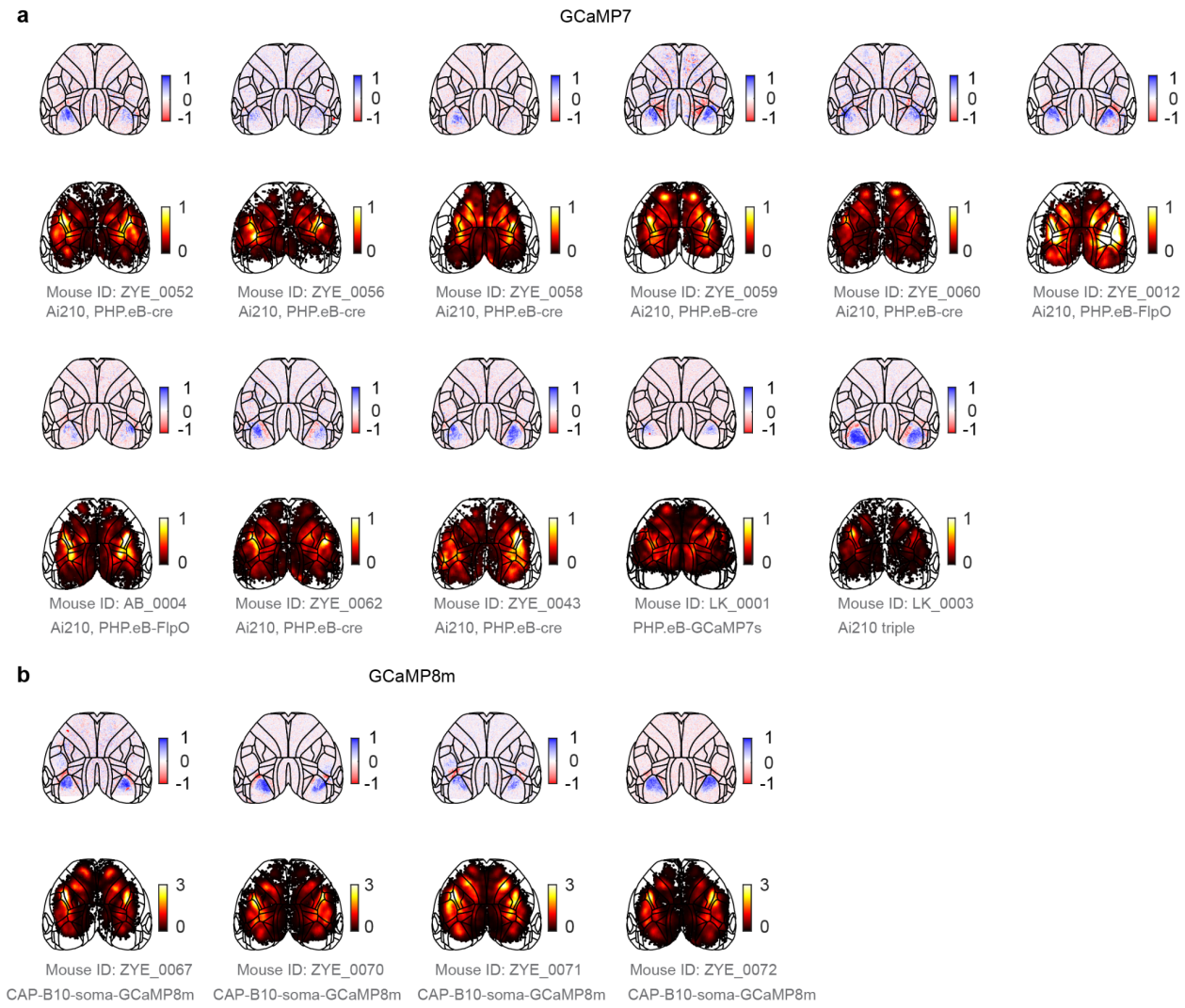
Extended Data Fig.3| Peak spiral density exceeded fourier phase shuffled control for spirals greater than or equal to 0.69 mm radius. Spirals could occur randomly within spatiotemporally correlated data. To evaluate whether the spirals we observed within the cortex were above chance level, we constructed shuffled Fourier phase surrogate data through the 3D fast Fourier transform (FFT) from raw data (x,y,t). We shuffled the phase values of the Fourier components, and created surrogate data by the inverse Fourier transform of the components from raw data with shuffled phases. By doing this, we

were able to preserve the spatial and temporal autocorrelation (or power spectrum) of the raw data. We then applied the same spiral detection algorithm to surrogate data. Spiral distributions were then compared between raw data and surrogate data across sessions. **a**, Example sequence of widefield raw trace (top row) and phase map (bottom row). To avoid including the field of view in FFT analysis that was outside of the brain, we drew a rectangle square to cover most of the posterior brain, but avoided the anterior brain. **b**, Sequence of surrogate data trace (top row) and phase map (bottom row). Surrogate data was constructed with 3D-FFT phase shuffling from the same section of data in **a**. **c**, Spiral density plots across 10 different spiral radius bins (from 0.17 mm to 1.73 mm at 0.17 mm steps). Top rows: All spirals detected and concatenated from raw data across 15 mice. Bottom rows: All spirals detected and concatenated from surrogate data across 15 mice. Density plots from raw data and phase scrambled data for the same radius were plotted at the same color scale for comparison. Spirals were highly concentrated within the center of SSp across all radius bins. **d**, Peak spiral density values within the SSp were compared between raw data and surrogate data across 15 mice for all 10 radius bins (0.17 mm:0.17 mm:1.73 mm). While peak density values for the first 3 small radius bins (0.17 mm, 0.35 mm, 0.52 mm) in the raw data (R) were not significantly different from the surrogate data (S), peak spiral density values significantly exceeded the surrogate data for larger radius bins (from 0.69 mm to 1.73 mm, at 0.17 mm steps). Each dot represents a single session from each of 15 mice. **e**, Peak spiral density values were compared between raw data and surrogate data with percentage change. Spiral density significantly increased from 46.7 ± 11.7% to 141.3 ± 16.9% , for spiral radius from 0.69 mm to 1.73 mm.

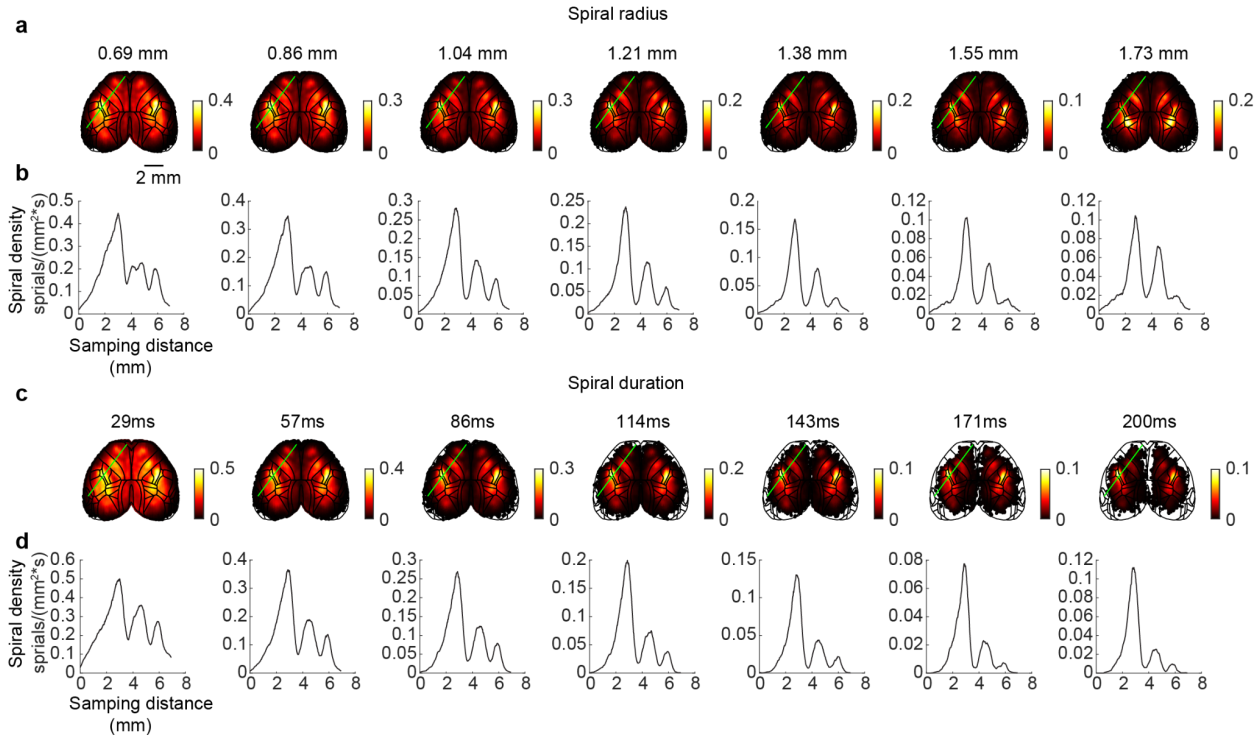


Extended Data Fig.4| Spirals in LFP activity with 4 shank Neuropixels recordings in the sensory cortex of a wide type C57BL/6 mouse. a, A 4-shank Neuropixels probe was programmed to be double-column per shank with 48 sites each column spanning 0.7 mm in length, and was inserted in a

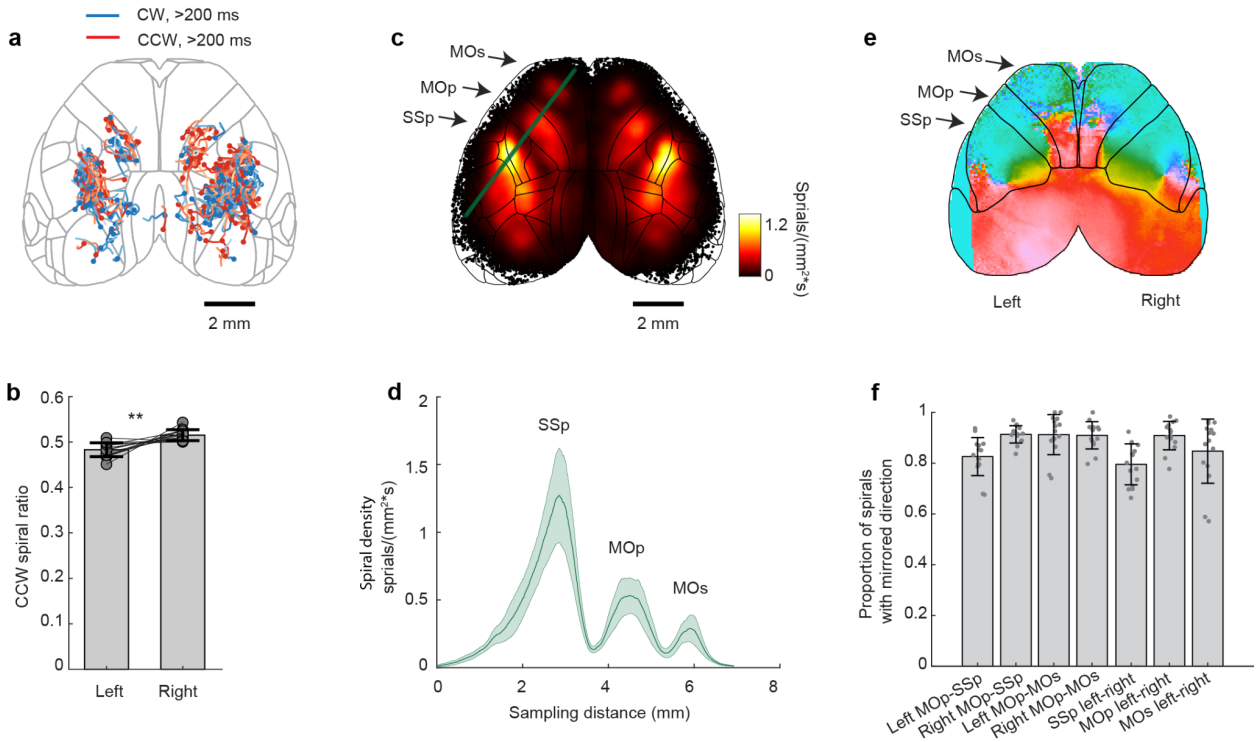
shallow angle to cover a large area of the sensory cortex in a wild type C57BL/6 mouse. **b**, LFP amplitude of the 4-shank Neuropixels probe was filtered at 2-8 Hz and downsampled to 35 Hz. Probe columns were compressed to a 2d map for visualization. The probe dimension with 4-shanks was 0.7 mm depth x 2.25 mm width. **c**, Phase values of filtered LFP trace at each site were extracted with the Hilbert transform, and phase map was constructed. **d**, An example of 0.5s LFP map. **e**, Phase map of 0.5s LFP activity in **d**. Note that spirals were observed in multiple frames of the 0.5s sequence.



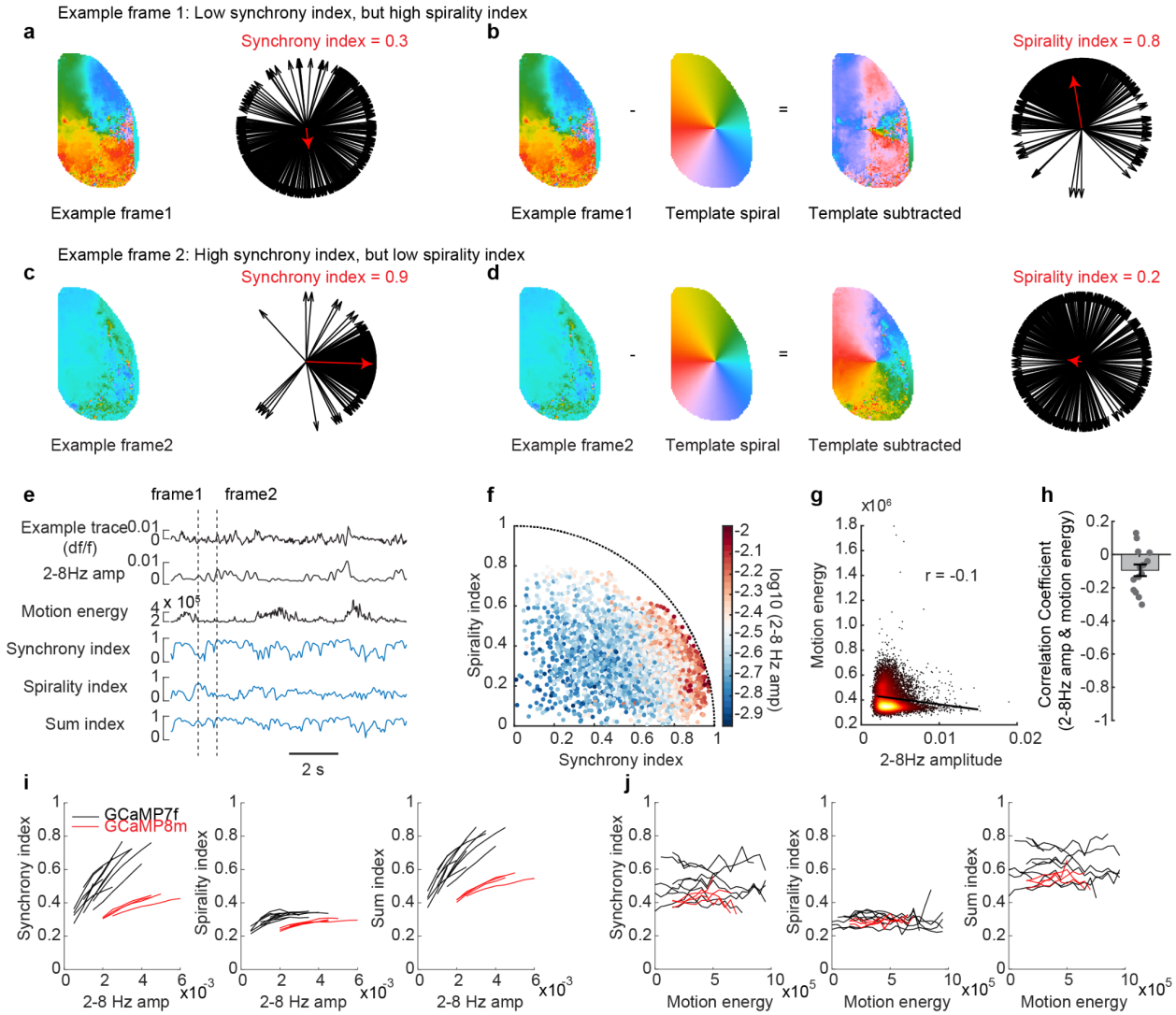
Extended Data Fig.5| Brain registration and spiral distribution across all GCaMP7 and GCaMP8m mice. a, Top: Brain atlas registration with visual field sign map as reference. Color bar: sign values within [-1, 1] range. Bottom: Spiral center density for all 11 GCaMP7 mice. Units: spirals/(mm^2*s). **b**, Same as **a**, but for 4 soma-GCaMP8m mice. GCaMP8m mice had significantly higher peak spiral rate at the center of SSp in comparison to GCaMP7 mice (GCaMP7: 0.8 ± 0.2 spirals/(mm^2*s), mean ± STD, 11 mice; GCaMP8m: 3.5 ± 0.6 spirals/(mm^2*s), 4 mice; $p = 7.7 \times 10^{-9}$,two-sample student's t-test).



Extended Data Fig.6| Consistent spiral distribution at different spiral radius and duration. a, All spirals from 15 mice were combined and sorted into different radius bins from 0.69 mm to 1.73 mm at 0.17 mm steps. The spiral density peaks at the center of SSp were consistent across different spiral radii. The separation of spiral peaks between SSp, MOp, and MOs were prominent across spiral radius bins. **b**, All spirals from 15 mice were combined and sorted into different duration bins from 28.6 ms to 200 ms at 28.6 ms steps. The spiral density peaks at the center of SSp, MOp, and MOs were consistent across spirals that fell within different sequence durations.

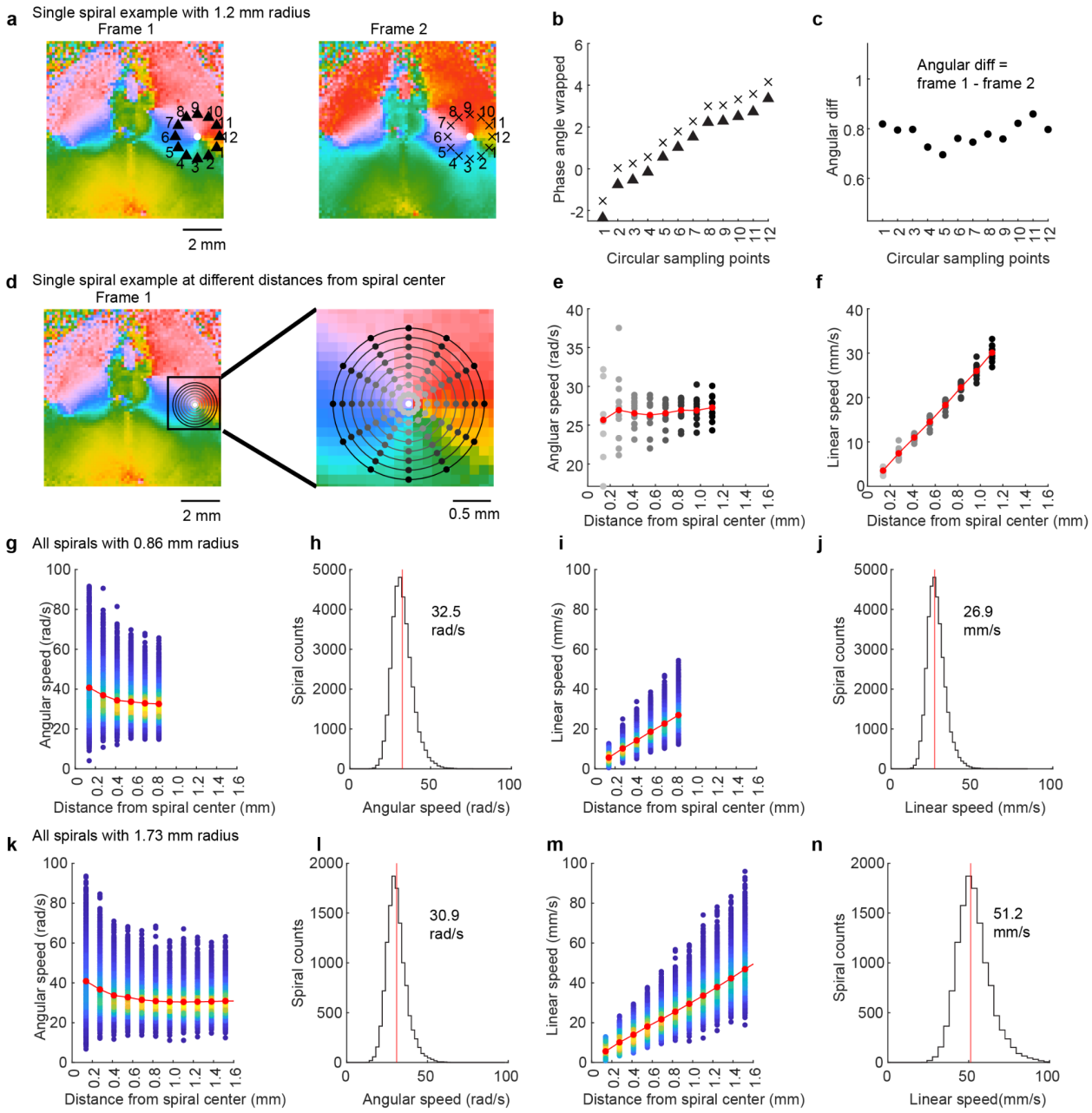


Extended Data Fig.7| Spiral traveling direction and distribution symmetry. a, Spiral centers smoothly drift over space and time. Example spiral center sequences that lasted longer than 200 ms in one example session are overlaid on the brain surface. Blue indicates clockwise traveling, red indicates counterclockwise traveling. The starting position of the sequence is indicated as a solid circle. **b**, Spiral sequences can travel both clockwise and counterclockwise. Spirals in the right hemisphere were slightly but significantly more likely to be counterclockwise traveling than spirals in the left hemisphere across mice. CCW spiral ratio in the left hemisphere: 0.46 ± 0.04 (mean ± STD); CCW spiral ratio in the right hemisphere: 0.54 ± 0.04 (mean ± STD); n = 15 mice, Student's t-test, $p = 1.5 \times 10^{-3}$. **c**, Spiral density distribution, summarized across all 15 mice. A line was drawn (green) to sample spiral density values across the SSp, MOp and MOs in the left hemisphere. **d**, Spiral density at green sampling points in **c** illustrates 3 peaks of spirals, centered in the SSp, MOp and MOs, consistent across mice (peak density at 1.3 ± 0.3 spirals/ (mm^2*s), n = 15 mice, mean ± SEM). **e**, Example spiral frame with region outline overlaid. **f**, Spirals detected on neighbor mirroring structures are mostly traveling in opposite directions. Each dot represents a session from each of 15 mice. Proportion of spirals with mirrored direction is the proportion of total frames with a pair of opposite spirals out of total frames with a candidate pair of spirals on mirroring structures. Left MOp-SSp: 82.6 ± 7.5% (mean ± STD); Right MOp-SSp: 91.3 ± 3.4%; Left MOp-Mos: 91.2 ± 7.9%; Right MOp-MOs: 91.0 ± 5.4% SSp left-right: 80.0 ± 8.0%; MOp left-right: 90.9 ± 5.6%; MOs left-right: 84.7 ± 12.7% (n = 15 mice).

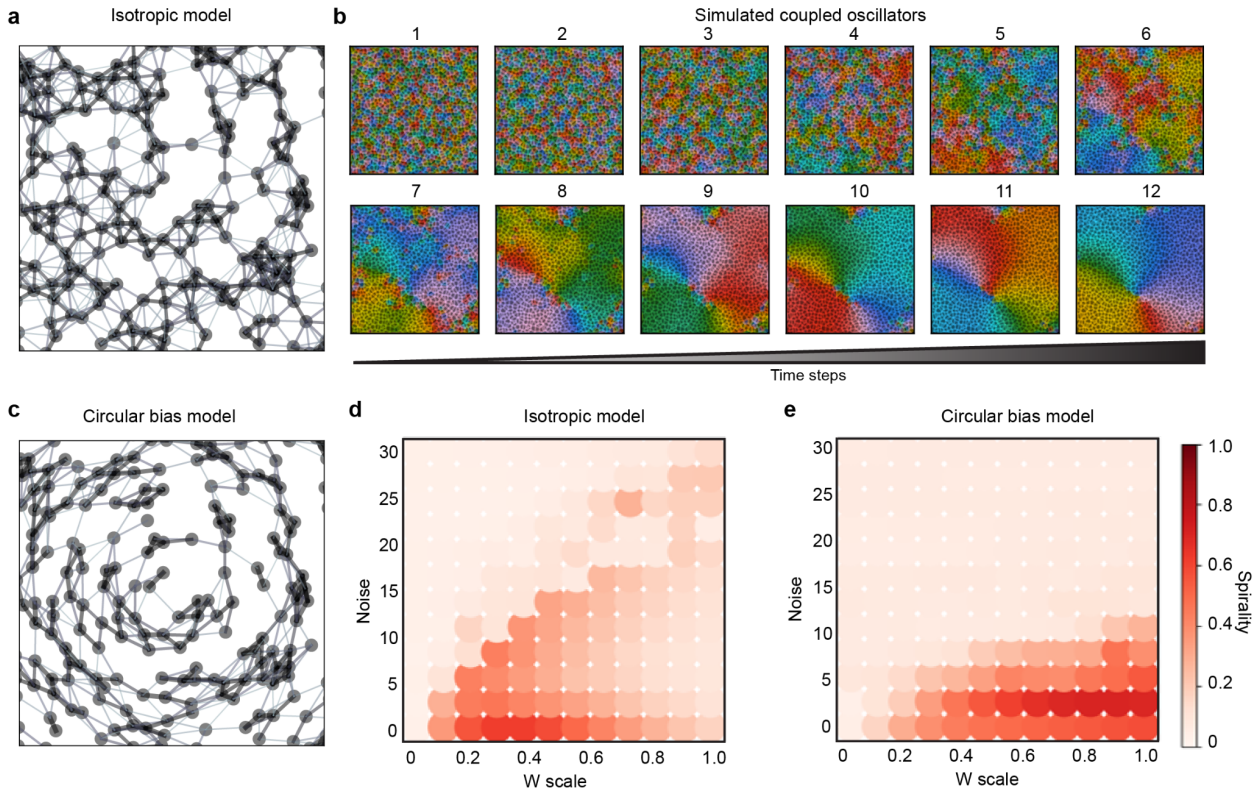


Extended Data Fig.8| Phase synchrony and spirality index increased as 2-8 Hz oscillation amplitude increased. **a**, Phase values across pixels in the example frame 1 had close to evenly distributed phase values from -π to π, which resulted in a synchrony index close to 0. **b**, However, for the same frame 1, while its synchrony index was close to 0, it had a spirality index closer to 1, indicating it had a spiral-like pattern. **c**,**d**, Example frame 2 has a synchrony index close to 1, but a spirality index close to 0. **e**, Time series of an example widefield cortical activity trace, mean 2-8 Hz amplitude, motion energy of the mouse face recording, synchrony index, spirality index and sum index for the right hemisphere of an example recording session (see Methods). Sum index = $\sqrt{Rsync^2 + Rspiral^2}$, which is also bounded between 0 and 1. Note that frames that had high synchrony index often had low spirality index, vice versa. Frame examples 1 and 2 in **a**-**d** are highlighted in the time series with dashed lines. Facial motion energy was the cross-pixel sum of absolute difference between consecutive frames of the mouse face video. **f**, Scatter plot of synchrony index and spirality index for each frame of a 100s epoch in the same session as in **e**. Each dot is color coded by the mean 2-8 Hz amplitude frame-to-frame. Frames with high mean 2-8 Hz oscillation amplitude had either high synchrony index or high spirality index. However, the distance of the dot to origin (sum index) is below 1, as shown with the dashed circular boundary. **g**, Scatter plot of 2-8 Hz amplitude and facial motion energy of an example session. 2-8 Hz amplitude was slightly negatively correlated with facial motion energy (r = -0.1). **h**, Pearson correlation

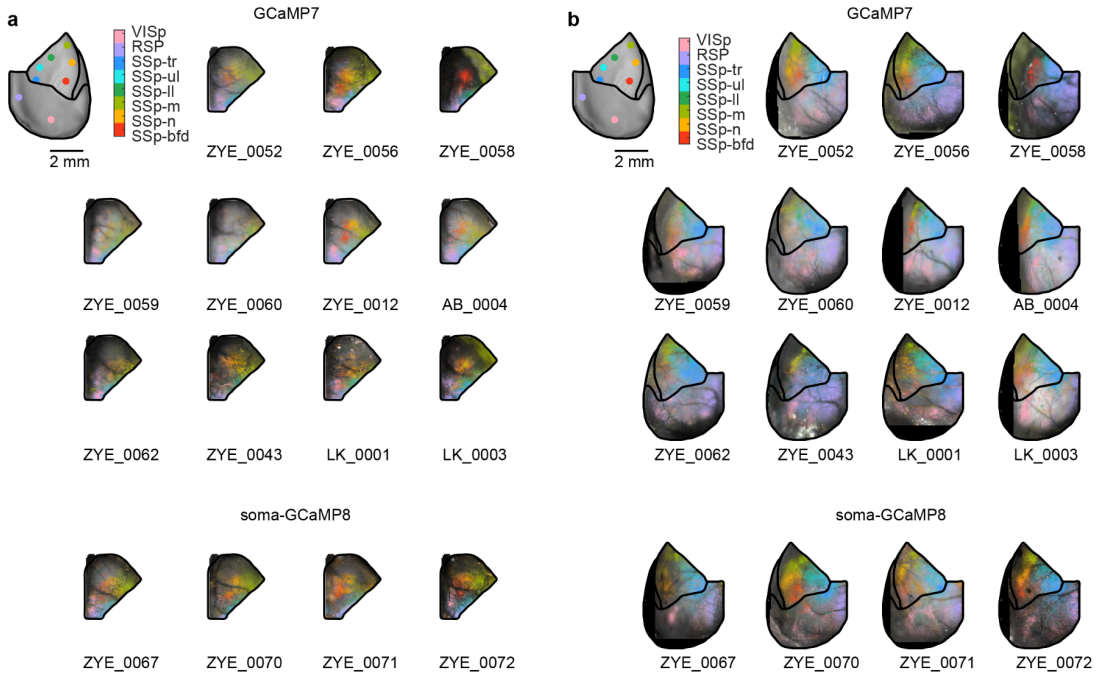
coefficient between 2-8 Hz amplitude and facial motion energy across 15 mice (r = -0.1 ± 0.04, Mean ± SEM). **i**, Mean synchrony index (left), spirality index (middle) and sum index (right) at different 2-8 Hz oscillation amplitude bins for a random 100s epoch across 15 mice. All index values increased as 2-8 Hz oscillation amplitude increased. Distributions of 2-8 Hz amplitude in GCaMP8m mice exhibited higher 2-8 Hz amplitude overall in comparison to GCaMP7 mice, presumably due to faster rise and decay kinetics resolving 2-8 Hz range oscillation better. **j**, Mean synchrony index (left), spirality index (middle) and sum index (right) at different motion energy bins of the mouse face recordings. Note there is no tendency of change of index across different motion energy bins, in comparison to 2-8 Hz amplitude bins in **i**, likely due to the weak correlations between 2-8 Hz amplitude and facial motion energy as shown in **g**,**h**.



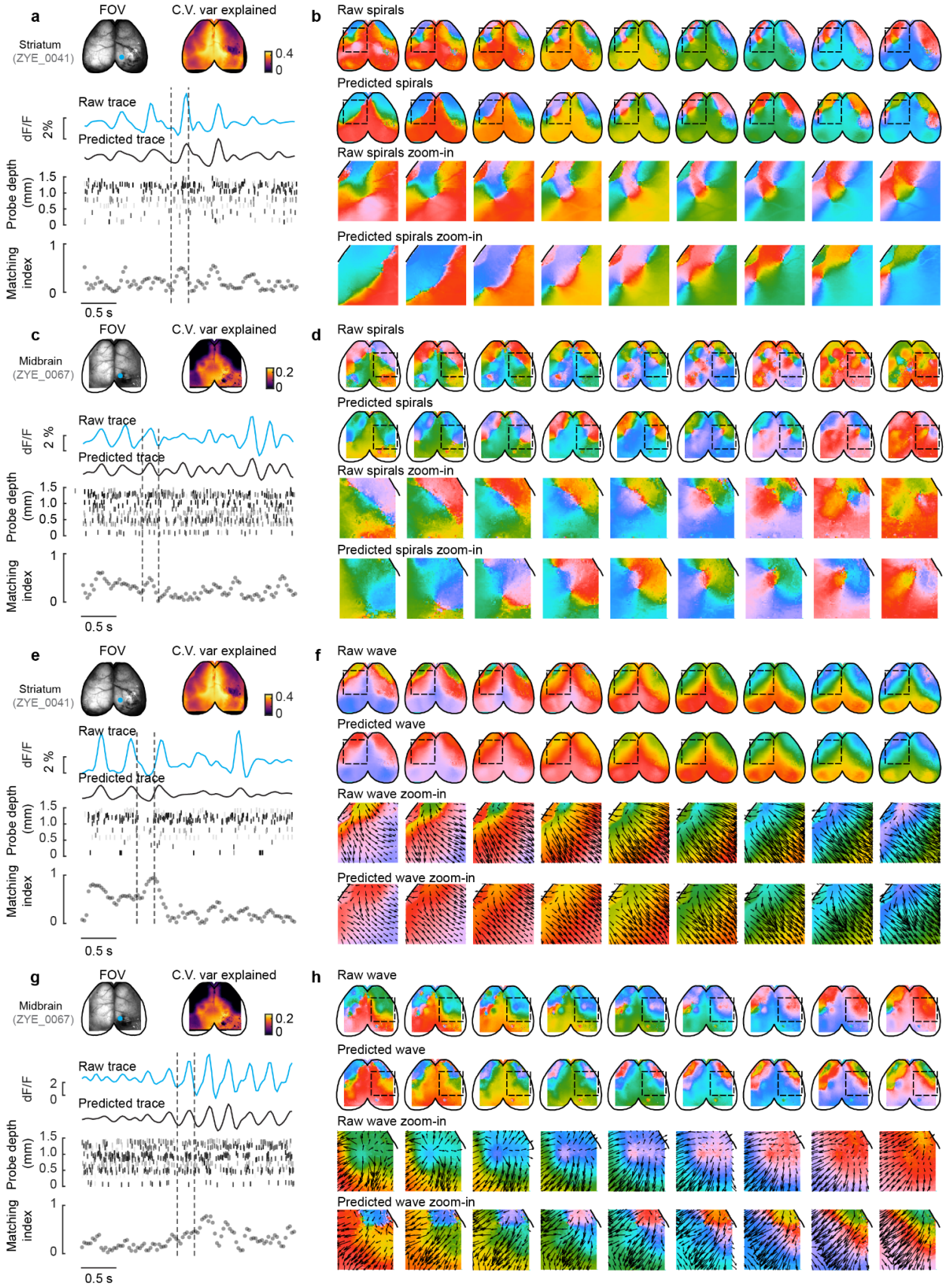
Extended Data Fig.9| Angular speed and linear speed calculation for spirals. To avoid the estimation errors of speed from optimization methods such as optical flow, we took advantage of the fact that spiral center coordinates and radius were automatically detected through detection pipeline (see Methods). Angular speed (ω) for a given pixel within the spiral is the angular displacement between 2 nearby frames, while linear speed (v) equals to radius (r) * angular speed (ω). **a**, Left: An example frame with spiral center and 12 evenly sampled points at spiral maximum radius (1.2mm) overlaid on top of the spiral frame. Right: Next frame after frame on the left. **b**, Phase angles from the 12 evenly sampled points in frames in **a** were unwrapped to eliminate phase discontinuities. **c**, Angular differences /displacements between the 2 example frames were consistent across all 12 sampling points. Angular speed (rad/s) is the product of angular difference between 2 frames (rad/frame) and frame rate (35 fps). **d**, Left: Sampling points with incremental distances from the spiral center, up to the maximum radius detected. Right: Zoom in on the spiral center. **e**, Angular speed (rad/s) for 12 evenly sampled points at incremental distances from the spiral center, up to the maximum radius detected. Different shades of gray color represent different distances from the spiral center as shown in **d**. Mean angular speed at different distances from the spiral center are overlaid in red. **f**, Linear velocities calculated from angular velocities in **e**. Mean linear velocities at different distances from the spiral center are overlaid in red. **g**, Angular speed density plot for all spirals with 0.86 mm maximum radius detected in all 15 mice, within an 1.7x3.4mm square close to the center of SSp in the right hemisphere. Mean angular speed of all spirals at different distances from the spiral center are overlaid in red. The slight increase in angular speed at a small distance from the spiral center may reflect an increased contribution of noise to these points. **h**, Angular speed histogram for all spirals with 0.86 mm maximum radius at maximum radius distance. **i**, Linear speed for all spirals with 0.86 mm maximum radius detected in all 15 animals. Mean linear speed of all spirals at different distances from the spiral center are overlaid in red. **j**, Histogram of linear speed for all spirals with 0.86 mm radius at maximum radius distance. **k**-**n**, Same as **g**-**j**, but for all spirals with 1.73 mm maximum radius detected in all 15 mice.



Extended Data Fig.10| Circular connectivity stabilizes spiral waves in a model of coupled oscillators. a, Illustration of the connectivity in an isotropic model. A network of coupled oscillators with local connectivity, but no circular bias, was generated to simulate network oscillations with the Kuramoto model (Methods). **b**, An example simulation exhibiting evolution of phase values from a randomized initial condition to spiral pattern over time. Node positions are plotted with a Voronoi graph. Consistent with previous results[78], traveling waves naturally emerged within such locally connected networks. **c**, Illustration of a circular bias model (Methods), with enhanced circular connectivity around a centerpoint. **d**, Spirals emerged within intermediate values of effective coupling strength (weight scale, w) and noise level in the isotropic model. Spiral waves were characterized with a spirality index (0 no spiral, 1 spiral-like) in the baseline isotropic model for spatially coupled oscillators (Methods). Across 1000 simulations (robust against 10 random seeds), spiral waves are more likely to be observed near the transition between a desynchronized regime and a synchronized regime, consistent with BKT transition theory[80,81]. **e**, Spirals are stabilized even at high weight scale (w) in the circular bias model. With circular connectivity bias σ at 50, spirals were significantly stabilized even at larger mean connectivity strength in comparison to the isotropic baseline.



Extended Data Fig.11| Activity kernel maps were consistent across sessions for motor-to-sensory cortex prediction and left-to-right hemisphere prediction. a, Kernel maps from n=15 mice showing motor-to-sensory cortex predictions for example pixels (filled dots) in the sensory cortex. Top 11 mice: GCaMP7f, bottom 4 mice: GCaMP8s. To account for the fact that fluorescence in GCaMP7s-expressing mice could arise in principle from both somas and axon terminals, we also tested subjects with soma-restricted GCaMP8m expression, which had similar results. **b**, Same as in **a**, but for 15 kernel maps from left-to-right hemisphere predictions.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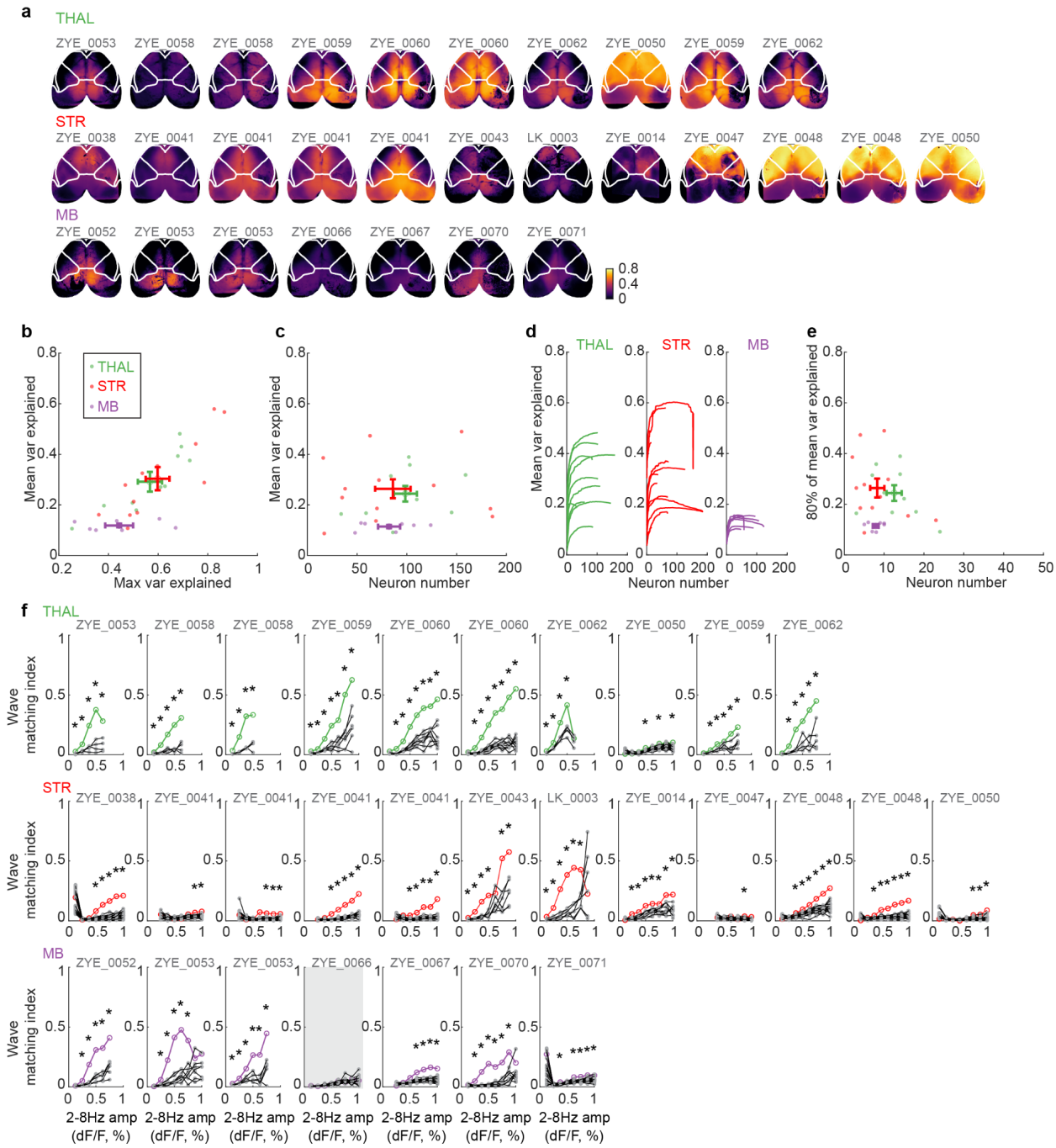
Extended Data Fig.12| Example spiral and traveling wave predictions from subcortical spiking activity. a, Example epoch of cortical spiral prediction from striatal spiking activity. Top row left: Mean intensity frame of widefield field of view (FOV). Note that the penetration position of the 4-shank Nueropixels probe was from the posterior cortex in the right hemisphere. Top row right: Cross-validated variance explained map of the cortical data from prediction with striatal spiking activity. Second row: Example raw (blue) and predicted (black) cortical activity trace in the example pixel, as indicated in the widefield FOV on the top row (blue dot). Third row: Raster plot of the spiking activity recorded from the Neuropixels probe. Spikes from all 4 shanks were concatenated, and ordered from bottom to top by the depth of the probe from the tip (0 mm) to the surface of the probe correspondingly. Each neuron was color coded by a randomized shade of gray color. Bottom row: Frame-to-frame traveling wave matching index. Note a general increase of wave matching index as 2-8 Hz amplitude increased. **b**, Example phase maps of the raw (top row) and predicted (second row) cortical activity within the dashed line in **a,** and the zoom-in of spirals in raw (third row) and predicted (fourth row) phase maps. **c**, **d**, Same as in **a**, **b**, but for an example midbrain recording session. **e**, Example epoch of cortical traveling wave prediction from striatal spiking activity. Same session as in **a**, but in a different time epoch. **f**, Example phase maps of the raw (top row) and predicted (second row) cortical activity within the dashed line in **e,** and the zoom-in of the raw (third row) and predicted (fourth row) phase maps and traveling waves, quantified with optical flow (Methods). Note that the directions of the raw and predicted traveling waves were similar, which were quantified as high traveling wave matching index in **e**. **g**,**h**, Same as in **e**,**f**, but for an example midbrain recording session. Same session as in **c**, but in a different time epoch.



Extended Data Fig.13| Prediction of cortical widefield activity and traveling waves from subcortical spiking activity. a, Cross-validated variance explained maps for cortical prediction from spiking data in three different subcortical regions. Top: thalamus; middle: striatum; bottom: midbrain. **b**, Mean variance explained were significantly higher for predictions from thalamic and striatal recordings than midbrain recordings (thalamus: 29.2 ± 3.9%, 10 sessions; striatum: 30.4 ± 4.6%, 12 sessions; midbrain: 11.9 ± 0.7, n = 7 session; mean ± SEM; thalamus vs striatum, p = 0.85; thalamus vs midbrain, p = 0.002; striatum vs midbrain, p = 0.007; Student's t-test, p<0.05). Peak variance explained for all three regions were not significantly different (thalamus: 56.7 ± 4.9%; striatum: 59.8 ± 4.8%; midbrain: 44.3 ± 5.6%; mean ± SEM; thalamus vs striatum, p = 0.66; thalamus vs midbrain, p = 0.12; striatum vs midbrain, p = 0.06; Student's

t-test, $p<0.05$). **c**, Total number of neurons recorded were not significantly different for all three subcortical regions (thalamus: 99 ± 12 neurons; striatum: 86 ± 18 neurons; midbrain: 82 ± 11 neurons; mean ± SEM; thalamus vs striatum, $p = 0.58$; thalamus vs midbrain, $p = 0.34$; striatum vs midbrain, $p = 0.88$; Student's t-test, $p<0.05$). **d**, Cumulative variance explained for cortical activity prediction from spiking data in three subcortical regions, ordered by contributions of each single neuron. Left: thalamus; middle: striatum; right: midbrain. In the first round of iteration for each session, cortical widefield activity was first predicted from each single neuron separately, and neurons were then sorted in descending order based on each neuron's contribution to variance explained. In the second round of prediction iteration for the same session, numbers of neurons used for prediction cumulatively increased from 1 to maximum number of neurons based on the contribution order established earlier, and cross-validated variance explained were calculated for each increment. Note that, in some sessions, variance explained starts to decrease after plateau, as neurons in the bottom contribution ranks start to add noise to full prediction with overfitting. **e**, Numbers of neurons accounting for 80% of peak cross-validated variance explained in **d** were not significantly different for all three subcortical regions (thalamus: 13 ± 2 neurons; striatum: 8 ± 2 neurons; midbrain: 8 ± 1 neurons; mean ± SEM; thalamus vs striatum, $p = 0.12$; thalamus vs midbrain, $p = 0.07$; striatum vs midbrain, $p = 0.87$; Student's t-test, $p<0.05$). Therefore, the lower variances explained from midbrain recordings were likely not due to different numbers of neurons recorded. **f**, Wave matching indexes increased as 2-8 Hz amplitude increased, and were significantly above permutation control (Thalamus: 10/10 session; Striatum: 12/12 session; midbrain: 6/7 sessions; unbalanced Two-Way ANOVA test, $p<0.05$). Session that failed the significance test is highlighted in gray. As examples above demonstrated (Extended Data Fig.12), wave matching indexes were high when 2-8Hz amplitudes were high. To quantify this relationship, we binned frames based on the mean 2-8 Hz amplitude in the raw cortical widefield data, and calculated the wave matching index from all frames within the amplitude bins. When original and predicted cortical wave directions, quantified with optical flow, matched well for the majority of pixels in frames from a given 2-8 Hz amplitude bin, wave angular difference values amongst all pixels between raw and predicted optical flow were uniformly distributed with low circular variance (close to 0), resulting in a matching index (1-circular variance) close to 1; when original and predicted cortical wave directions did not match, angular difference values were spread out with high circular variance (close to 1), resulting in a matching index (1-circular variance) close to 0. For permutation tests, unit identities were shuffled in the test dataset for 20 times without retraining the model, before optical flow and matching indexes were calculated. If the oscillation phase of different units within the subcortical areas were uniform, or random without extra information, measured matching index distribution should not be significantly different from shuffled permutations.