Spatially and Blood Flow-Dependent Tissue Distribution of Thyroid Hormones by Plasma

Thyroid Hormone Binding Proteins

Running title: Modeling Thyroid Hormone Binding Proteins

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Abstract

Plasma thyroid hormone (TH) binding proteins (THBPs), including thyroxine-binding globulin (TBG), transthyretin (TTR), and albumin (ALB), are important in regulating thyroxine (T4) and triiodothyronine (T3). THBPs carry THs to extrathyroidal sites, where THs are unloaded locally and then taken up via membrane transporters into the tissue proper. The respective roles of THBPs in supplying THs for tissue uptake are not completely understood. To investigate this question, we developed a spatial human physiologically based kinetic (PBK) model of THs, which produces several novel findings. **(1)** Contrary to postulations that TTR and/or ALB are the major local TH contributors, the three THBPs may unload comparable amounts of T4 in *Liver*, a rapidly perfused organ; however, their contribution in *Rest-of-Body (RB)*, which is more slowly perfused, follows the order of abundance of T4TBG, T4TTR, and T4ALB. The T3 amounts unloaded in both compartments follow the order of abundance of T3TBG, T3ALB, and T3TTR. **(2)** Any THBP alone is sufficient to maintain spatially uniform TH tissue distributions. **(3)** The TH amounts unloaded by each THBP species are spatially dependent and nonlinear in a tissue, with ALB being the dominant contributor near the arterial end but conceding to TBG near the venous end. **(4)** Spatial gradients of TH transporters and metabolic enzymes may modulate these contributions, producing spatially invariant or heterogeneous TH tissue concentrations depending on whether the blood-tissue TH fluxes operate in near-equilibrium mode. In summary, our modeling provides novel insights into the differential roles of THBPs in local TH tissue distribution and homeostasis.

Key words: Thyroid hormone, Thyroxine-binding globulin, Transthyretin, Albumin, Tissue distribution, Gradient

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 Introduction

The circulating thyroxine (T4) and triiodothyronine (T3) levels are robustly regulated to stay

within narrow (about 2-3 fold) physiological ranges (Jain 2015, Welsh and Soldin 2016).

Deviations of the thyroid hormones (THs) from the normal ranges lead to a variety of adverse

health outcomes (Combs et al. 2011, Jabbar et al. 2017, Prezioso et al. 2018, Silva et al. 2018,

Yavuz et al. 2019). By maintaining the setpoint levels of THs, the hypothalamic-pituitary-thyroid

(HPT) axis is the primary mechanism for long-term TH homeostasis. To combat transient

perturbations, it requires three major TH binding/distributor proteins (THBPs/THDPs) in the

blood: thyroxine-binding globulin (TBG), transthyretin (TTR), and albumin (ALB).

The vast majority of circulating THs are bound to and transported by these THBPs

(Janssen and Janssen 2017, McLean et al. 2017), with a small fraction also bound to

lipoproteins and members of the serine proteinase inhibitors (serpins) superfamily (Benvenga et

al. 1988, Benvenga et al. 2002, Benvenga 2013). The molar abundances of the three THBPs in

humans follow the order of ALB>TTR>TBG, with ALB more than a hundred times higher than

TTR and TTR more than tens of times higher than TBG (Attwood et al. 1978, Gardner and Scott

1980, Attwood and Atkin 1982, Vatassery et al. 1991). However, the binding affinities of THs for

the three THBPs follow the reverse order: TBG > TTR > ALB. The binding affinities of T4 for the

three THBPs differ by more than two orders of magnitude, while in the case of T3, the binding

affinities differ by at least one or two orders of magnitude (Murata et al. 1985, Yabu et al. 1987,

Chang et al. 1999, Richardson 2007, McLean et al. 2017). As a result of the vast differences in

the THBP abundances and binding affinities, TBG accounts for ~75% of both plasma total T4

and total T3 despite its low abundance and having only one binding site, TTR accounts for

~15% of total T4, but less than 5% of total T3, and ALB accounts for less than 5% of total T4

and ~20% of total T3 (Schussler 2000, Janssen and Janssen 2017, McLean et al. 2017).

Overall, less than 0.03% of plasma T4 is free with the vast majority bound to THBPs, while

about 0.3% of plasma T3 is free with the vast majority also bound to THBPs (Mendel 1989,

Richardson 2007, McLean et al. 2017). TBG is only about 20% saturated and TTR is less than

1% saturated by THs with the majority of their binding sites unoccupied by THs (Schussler

2000, McLean et al. 2017). THBPs are believed to have several functions. (1) They produce a

strong buffer in the plasma where a transient increase or decrease of free T4 and T3 can be

quickly dampened. (2) THs stored in THBPs can act as a reservoir in the face of short-term TH

deficiency. (3) THBPs are required to ensure uniform distribution of circulating THs through a

perfused tissue; in the absence of THBPs, a steep gradient of tissue THs would result (Weisiger

et al. 1986, Mendel et al. 1987, Mendel et al. 1988).

While a lot has been learned about THBPs, many questions remain unanswered. THs

are taken up by tissues in free form mainly via cell membrane transporters including MCT8,

MCT10, LAT1, LAT2, OATP1c1 etc. (Pizzagalli et al. 2002, Friesema et al. 2003, Bernal et al.

2015, Zevenbergen et al. 2015, Groeneweg et al. 2020). However, the bulk of these free THs

that move into the tissues must first be unloaded off of THBPs in the tissue capillary. The

relative contributions of each THBP species in this regard are not completely established but

are important for understanding TH tissue distribution as well as potential species differences in

TH kinetics. It has been speculated that because of the faster dissociation rate constants for the

binding between THs and ALB (i.e., shorter residence time of T4 and T3 on an ALB molecule),

ALB contributes the most THs to the perfused tissues (Mendel 1989, Schussler 2000). It is also

argued that TTR may be the one that contributes the most T4 to tissues because of its

"Goldilocks" (just-about-right) properties among the three THBPs, i.e., intermediate abundance

and binding affinity (Robbins 2002, Richardson 2009, Alshehri et al. 2015). Given that TBG is

loaded with over two thirds of total T4 and total T3 in the blood, it is also possible that this high

abundance compensates for its tight grip on THs such that it makes comparable or even greater

contributions than ALB and TTR. In addition, the blood perfuses different tissues at different flow

rates, thus THBPs carrying THs would clear through tissues in different amounts of time, during

which free THs transport into and out of tissues at potentially different rates. It is unclear how all

these factors – the residence time of THs on THBPs, THBP abundance, tissue blood transit

time, as well as the rates of blood-tissue TH exchange – interplay to determine the amounts of

THs that are unloaded from each THBP species in local tissue blood and eventually move into

the tissue proper.

While ingenious experimentation can help clarify many of these questions, quantitative

understanding of the thyroid system can also benefit greatly from mathematical modeling

(DiStefano and Chang 1971, Oppenheimer and Schwartz 1985, Pilo et al. 1990, Curti and

Fresco 1992, Eisenberg et al. 2008, McLanahan et al. 2009, Lumen et al. 2013, Berberich et al.

2018, Handa et al. 2021). A physiologically based kinetic (PBK) model of THs containing

sufficient details of the THBP binding events with spatial configurations will help dissect the

differential roles of THBPs and provide critical quantitative insights. Here we developed a spatial

human PBK model of THs based on a nonspatial model we have recently published (Bagga et

al. 2023), and reported several novel findings on local TH tissue delivery and contributions by

different THBP species.

Methods

1. The nonspatial human PBK model of THs

The details of the nonspatial human PBK model of THs, including its construction and parameterization, were described in our recently published paper (Bagga et al. 2023). The model was rigorously parameterized based on numerous published studies on THBP binding affinities, association/dissociation rate constants, TH and THBP concentrations, plasma/tissue partitioning, half-lives, etc. Briefly, the model contains four major compartments: *Body Blood*, *Thyroid*, *Liver*, and *Rest-of-Body* (*RB*) (Fig. 1A). The *Liver*, *RB*, and *Thyroid* compartments contain respective tissue blood (vasculature) and tissue proper (extra-vasculature) subcompartments. In each blood (sub)compartments, the binding events between THs and THBPs follow the law of mass action (Fig. 1B). As standard PBK practices, here the concentrations of molecular species in *Body Blood* are treated as their arterial concentrations (CA), and the concentrations in tissue blood are treated as proxies for their venous concentrations (CVT, CVRB, and CVL) (Fisher et al. 2020). The model produced several novel findings, including fast and near-equilibrium blood-tissue TH exchanges as an intrinsic robust mechanism against local metabolic perturbation and tissue influx as a limiting step for transient tissue uptake of THs in the presence of THBPs (Bagga et al. 2023). Since we were concerned with the steady-state behaviors of THs in local tissues, it was not necessarily to include the feedback regulation of TSH by THs in the model, which is a simplification that is also applied to the spatial model presented below.

2. Construction of the spatial human PBK model of THs

In order to examine the gradients of TH distribution in tissues, we extended the nonspatial PBK model above into a spatial model. Specifically, the *RB* and *Liver* compartments are divided into 200 linear segments of equal size with each segment containing its own tissue blood and tissue proper subsegments (Fig. 1C). 200 segments provide a sufficient resolution to simulate the

concentration gradients as higher numbers of segments do not appreciably improve the

precision (simulation results not shown). The concentration of each molecular specie in the last

(200th) tissue blood subsegment is treated as its tissue venous blood concentration. Each

subsegment is assumed to be well-mixed and has its own set of ordinary differential equations

(ODEs) tracking the subsegment-specific rates of change of the variables. The method of lines

is used to track the molecular species in each subsegment. The ith and $i+1^{th}$ blood subsegments

are connected by the unidirectional blood flow of each molecular species. The kinetic constants

$k_1 - k_{12}$ for TH and THBP binding in the blood (i.e., the association rate constants and

dissociation rate constants) are assumed the same across all blood subsegments and equal to

the values in the nonspatial PBK model. The bidirectional transport of free T4 and free T3

between the tissue blood and tissue proper subsegments as well as T4-to-T3 conversion

metabolism and clearance metabolism within each tissue proper subsegment also occur as

described in the nonspatial PBK model. The parameters describing the influx and efflux within

each tissue segment (k_{21}, k_{23}, k_{25}, k_{27}, k_{28}, k_{29}, k_{30}, and k_{31}) are scaled from the values used in

the nonspatial PBK model by dividing by 200, the total number of segments. The parameters

describing the metabolism within each tissue segment (k_{24}, k_{26}, k_{32}, k_{33}, k_{34}, and k_{35}), which are

first-order rate constants, remain the same as in the nonspatial PBK model. For homogenous

simulations, the values of each of these parameters (k_{21}, $k_{23} - k_{35}$) are equal across all

segments. For heterogeneous simulations where a parameter value may vary from the arterial

to venous ends, a linear gradient was applied to each parameter across the segments such that

the average is equal to the constant value in the homogenous case.

One additional consideration is the possible bidirectional diffusion of molecular species

across the blood subsegments and across the tissue subsegments. The diffusion of a molecular

species would be normally modeled as $(species_{i-1} + species_{i+1} - 2 * species_i)/dx^2$ where i

represents the current subsegment, $i - 1$ the subsegment before, $i + 1$ the subsegment after,

and dx is the length of the subsegment. Since the diffusion rate is much slower than the blood

flow rate (Weisiger et al. 1986), including cross-subsegment diffusions didn't produce any

difference in the model's behavior based on our simulations (results not shown). Therefore, for

all spatial PBK simulations we proceeded without considering cross-subsegment diffusions.

3. Model parameters, equations, and simulation tools

Model parameter values and details of the source references and justifications, ordinary

differential equations (ODEs), and algebraic equations were described in (Bagga et al. 2023).

Both the nonspatial and spatial models were constructed in MATLAB R2019a (MathWorks

Natick, Massachusetts, USA), and *ode15s* was used to numerically solve the ODEs. All

MATLAB code is available at https://github.com/pulsatility/2023-TH-PBK-Model.git.

Results

Among the three THBPs, it has been argued that ALB and/or TTR play a larger role than TBG in

supplying THs to tissues because of their lower binding affinity for THs and/or shorter residence

time of T4 and T3 on these proteins (Mendel 1989, Schussler 2000, Robbins 2002, Richardson

2009, Alshehri et al. 2015). We explored this issue with both the nonspatial and spatial versions

of the PBK model below.

1. Nonspatial PBK model

1.1 TH unloading in *Liver blood*

Compared with the respective arterial concentrations, free T4 (*fT4*), *T4TBG*, *T4TTR*, and *T4ALB*

in the venous blood leaving the *Liver* compartment are only negligibly lower, dropping by 0.02%-

0.18% (Table 1). *fT4* drops by 0.18%, which is comparable to the percentage drop of *T4ALB*

(0.17%), however, *T4TTR* drops only by 0.069% and *T4TBG* by 0.022%. This result suggests

that only *T4ALB* is in near equilibrium with *fT4* as the blood transits through the *Liver*. Here,

equilibrium refers to the state when the rate of association between T4 (or T3) and either *TBG*,

TTR or *ALB* equals the rate of dissociation of the respective TH-THBP complex. The difference

in the percentage drops of these three T4-THBPs can be explained by the T4 residence time on

these proteins relative to the blood transit time through the *Liver*. Given the vascular volume and

blood flow rate of the *Liver* (Bagga et al. 2023), the blood transit time is about 8.3 seconds. The

average residence time of T4 on TBG, TTR and ALB, as determined by the inverse of the

dissociation rate constants k_2, k_4, and k_6, is 55.55, 12, and 0.77 seconds respectively.

Therefore, it is expected that *T4ALB* can unload quickly in response to the drop of *fT4* as *fT4*

moves into the *Liver tissue*, while *T4TTR* unloads much more slowly, and *T4TBG* unloads the

slowest during this short transit time. Despite these differences, the absolute amounts of T4

unloaded from the three THBPs are not much different – the concentration of *T4TBG* decreases

the most, by 15.2 pM, followed by *T4ALB*, 12.3 pM, and *T4TTR*, 11.8 pM. This is because

although the relative speed of T4 dissociation from TBG is much slower than from ALB, *T4TBG*

has a much higher (nearly 10 times) abundance than *T4ALB*, resulting in a higher absolute

amount of T4 unloaded in the *Liver blood* of the nonspatial model.

For T3 in *Liver*, the venous blood concentrations are negligibly lower than the arterial

concentrations by 0.24%-0.42% (Table 1). Free T3 (*fT3*) drops by 0.42%, comparable to the

percentage drop of *T3ALB* (0.4%), only slightly higher than *T3TTR* (0.36%), but tangibly higher

than *T3TBG* (0.24%). The average residence time of T3 on TBG, TTR and ALB, as determined

by the inverse of the dissociation rate constants k_8, k_{10}, and k_{12}, is 6.06, 1.45, and 0.45 seconds

respectively. Compared with the blood liver transit time of 8.3 seconds, it is clear that *T3ALB*

and *T3TTR* can reach near equilibrium with *fT3* during this time, while *T3TBG* can only partially

reach equilibrium. However, like the case of T4, *T3TBG* contributes the most T3 unloaded in the

Liver blood with an absolute drop of 3.0 pM, followed by 1.3 pM by *T3ALB*, and a much smaller

0.3 pM by *T3TTR*.

1.2 TH unloading in *RB blood*

For T4 in *RB*, the venous blood concentrations are negligibly lower than the arterial

concentrations by 0.017%-0.078% (Table 1). Similar to the case in *Liver*, the percentage drop of

T4ALB is comparable to that of *fT4*, while *T4TBG* drops by a much smaller fraction. Given the

vascular volume and blood flow rate of *RB* (Bagga et al. 2023), the blood *RB* transit time is 20

seconds, which is much longer than the T4 residence time on ALB, nearly twice as long as on

TTR, and less than half of the residence time on TBG. The absolute amounts of T4 unloaded

from the three THBPs are quite different, where *T4TBG* unloads the most by 11.8 pM, *T4TTR*

the second by 7.5 pM, and *T4ALB* the least by 5.6 pM.

For T3 in *RB*, the venous blood concentrations are negligibly lower than the arterial

concentrations by 0.062%-0.088% (Table 1). *fT3* drops by 0.088%, similar to that of *T3ALB* and

T3TTR, and only slightly higher than that of *T3TBG* (0.062%), which can be explained by the

much longer blood *RB* transit time than the residence times of T3 on these THBPs (20 vs. 6.06,

1.45, and 0.45 seconds). Similar to T3 in *Liver*, *T3TBG* contributes nearly 70% of T3 unloaded

in *RB blood* with an absolute decrease of 0.78 pM, followed by 0.29 pM by *T3ALB*, and a much

negligible 0.07 pM by *T3TTR*.

2. Spatial PBK model

The nonspatial PBK model provides some preliminary insights into the relative contributions of

THBPs to local THs. A caveat of the nonspatial model is that the *Liver* and *RB* are treated as

well-mixed compartments, so it is unable to predict the concentration gradients of THs in the

tissues. To this end, we utilized the spatial PBK model, where both the *Liver* and *RB*

compartments are simulated as 200 interconnected, consecutive segments as detailed in

Methods (Fig. 1C). The half-lives of plasma T4 and T3 and the decay profiles in simulated T4 or

T3 tracer experiments, in either the presence or absence of THBPs, are nearly identical to the

nonspatial model (simulation results not shown).

2.1 Overall contributions of THBPs to TH unloading in tissue blood

The spatial PBK model predicts that the arterial and venous plasma concentrations of both T4

and T3 are marginally lower than the corresponding concentrations in the nonspatial PBK model

(Tables 2 vs. 1). For a given TH variable, the differences between the arterial and venous

concentrations are similar between the two models, and the relative contributions of TBG, TTR

and ALB to providing THs to the tissues are by and large in the same order as predicted by the

nonspatial model. One exception is *Liver* T4, where although the contributions of the three

THBPs are still comparable, ALB unloads (14.4 pM) 10% more than TBG (13.1 pM) does, while

in the nonspatial model TBG unloads 20% more than ALB does. The percentage contributions

by each THBP species in the spatial model are summarized in Fig. 2.

2.2 TH concentration gradients

The spatial plasma concentrations of *fT4* and the three T4-THBPs in tissue blood exhibit very

different gradient profiles (Fig. 3A-3E). *fT4* (Fig. 3A) and *T4ALB* (Fig. 3D) in both *Liver blood*

and *RB blood* show similar, exponential-like drops (with the exception that *fT4* exhibits a

discrete drop in the first segment). When examined on logarithmic scale of the Y axis, the

decays do not follow a straight line (results not shown), indicating that they are not truly

exponential. In contrast, *T4TBG* exhibits a decreasing trend that is concave downward (Fig. 3B),

while *T4TTR* is concave downward initially but then transitions to a nearly linear decay phase,

especially in *RB blood* (Fig. 3C). Interestingly, *Total T4* decays in a basically linear fashion (Fig.

3E). The concentration gradients of T4 in *Liver tissue* and *RB tissue* follow the same trend and

profile as *fT4* in the respective tissue blood, and the percentage drops from the first segment to

the last segment, which are negligibly small, are also the same as the drop of *fT4* (results not

shown). These gradient profiles are qualitatively similar in both the *Liver* and *RB* compartments,

but the concentration drops are generally steeper in *Liver* than in *RB*. The gradient profiles of T3

are similar to those of T4 (Fig. 3F-3J), except that *T3TTR* exhibits a concave-upward profile for

the most part (Fig. 3H) whereas *T4TTR* is more concave-downward (Fig. 3C).

2.3 Nonlinear, spatially dependent THBP unloading of THs in tissue blood

We next calculated the difference in T4-THBP concentrations between two consecutive tissue

blood segments, which represents the amount of T4 that is unloaded by the THBPs in the

downstream segment of the two. It is interesting to note that the concentration drop of each

THBP species varies depending on the location of the segments (Fig. 4A and 4B). ALB clearly

contributes the most T4 in the upstream *Liver* segments, but as the blood perfuses downstream,

the contributions by TBG and TTR start to catch up halfway through. Toward the venous end of

the *Liver* compartment, TBG becomes the dominant contributor, TTR the intermediate contributor, and ALB the smallest contributor (Fig. 4A). A similar change of order in contribution between ALB, TBG and TTR also occurs in the *RB* compartment, although more upstream, nearly quarter-way through (Fig. 4B). Interestingly, the *T4TTR* drop exhibits a nonmonotonic profile in *RB*. The contributions of TBG and ALB to T3 unloaded in *RB blood* exhibit similar profiles to the case of T4, with changes in the order of contribution occurring at further upstream locations (Fig. 4C and 4D). *T3TTR* has the smallest contribution also showing nonmonotonicity in the *Liver blood* and *RB blood* compartments. At downstream locations in *RB*, the amount of T3 unloaded from each of the three THBPs seems to reach a constant.

This nonlinear, spatially dependent, differential TH unloading by the three THBPs is due, at least in part, to the differences in the residence time of T4 and T3 on the THBP molecules. In the upstream segments, for instance, as *fT4* moves into the tissue such that its local concentration drops, *T4ALB* releases T4 much more quickly than *T4TTR* and *T4TBG*. The T4 released by *T4ALB* likely further slows down the release of T4 from *T4TTR* and *T4TBG*, resulting in the concave-downward gradients of the two species (Fig. 3B and 3C). As the blood flows through the remaining segments downstream where *fT4* drops to lower levels, *T4TTR* and *T4TBG* are further removed from their equilibrium with *fT4* (Fig. 5A-5B and 5D-5E). This built-up "tension" or disequilibrium begins to force *T4TTR* and *T4TBG* to release more T4 than in the upstream segments. While in contrast, *T4ALB* moves further toward equilibrium, therefore releasing less T4 (Fig. 5C and 5F). The evolution of the binding disequilibrium between T3 and THBPs through tissue blood shows similar trends to the case of T4 (Fig. 6). *T3TTR* binding disequilibrium exhibits nonmonotonic changes in both *Liver blood* (Fig. 6B) and *RB blood* (Fig. 6E), similar to *T4TTR* in *RB blood* (Fig. 5E), which explains the bell-shaped contributions to T3 (Fig. 4C-4D) and T4 (Fig. 4B) by TTR.

The differential contribution to the amounts of THs unloaded in tissue blood by different

THBPs cannot be explained, however, solely by the difference in the residence time of T4 or T3

on THBP molecules. There is a quantitative mismatch. For instance, the residence time of T4 on

ALB is 70 times shorter than on TBG and nearly 16 times shorter than on TTR. However, in the

first segment of the *Liver*, *T4ALB* contributes only about 7 times higher T4 than *T4TBG*, and the

T4TBG contribution is on par with *T4TTR* contribution (Fig. 4A). An examination of the absolute

association rates and dissociation rates of all TH/THBP pairs reveals that the relative

contributions to THs unloaded by the three THBPs in the most upstream segments are basically

proportional to the absolute dissociation rates in the arterial blood (Figs. 5 and 6 and Table S1).

These dissociation rates are determined not only by the dissociation rate constant parameters

(which determine the residence time), but also by the concentrations of TH-THBP complexes. In

the case of contributions to the amount of T4 unloaded in local tissues, *T4TBG* and *T4TTR* have

higher concentrations than *T4ALB*, which compensate to a great extent their longer residence

time.

Despite the nonlinear, varying contribution by each of the three THBPs across tissue

segments, the total amounts of T4 and T3 unloaded by all three THBPs combined is highly

constant across tissue segments (Fig. 4, green lines). The amount of T4 unloaded and thus

delivered in the last segment is only 0.16% and 0.07% lower than that in the 1st segment in the

Liver and *RB* compartments respectively, and in the case of T3, the difference is 0.82% and

0.12% respectively. These results support the notion that THBPs play a crucial role in

maintaining a constant concentration and uniform delivery of THs through the tissues. This is

further demonstrated when all three THBPs are removed in the spatial model (Fig. 7). The

arterial concentration of *fT4* increases dramatically to 34 pM, compared with 15 pM when all

three THBPs are present, and the venous concentrations leaving the *Liver* and *RB*

compartments drop to 2.5 and 6.5 pM respectively, forming steep exponential gradients (Fig. 7A

and 7B, solid line). T4 concentrations in the *Liver tissue* and *RB tissue* follow a similar

descending gradient with nearly identical percentage drops as *fT4* (Fig. 7C and 7D, solid line).

The arterial concentration of *fT3* increases to 5.81 pM, compared with 5 pM when all three

THBPs are present. Surprisingly, unlike T4 which exhibits a monotonically descending gradient,

plasma *fT3* exhibits a bell-shaped gradient in both *Liver* and *RB* when all three THBPs are

absent (Fig. 7E and 7F, solid line). *fT3* first increases slightly less than 1/10th way through the

Liver blood, and then decreases in a nearly linear fashion followed by a slightly concave-upward

decay down to 1.76 pM (Fig. 7E). The bell shape of the plasma *fT3* gradient in *RB* is more

dramatic, where *fT3* first rises to 6.16 pM more than 1/5th way through the tissue, and then

decreases to 4.46 pM as it exits the tissue (Fig. 7F). T3 in *Liver tissue* follows a similar

nonmonotonic gradient profile as *fT3* in *Liver blood* (Fig. 7G, solid line) but T3 in *RB tissue* only

exhibits a monotonic decay (Fig. 7H, solid line). The nonmonotonicity of *fT3* gradients in the

tissue blood in the absence of all three THBPs is explained in Fig. S1.

The above results clearly demonstrate that THBPs are essential to maintain constant

concentrations and uniform delivery of THs through the tissues. We next examined if any one of

the three THBPs is sufficient to fulfill this function. When only either TBG, TTR, or ALB remains

in the model, the concentrations of T4 and T3 across the blood and tissue segments exhibit

negligible drops and the arterial concentrations are nearly identical to the concentrations when

all three THBPs are present (Figs. 8-10). The only notable changes are *fT3* concentration when

only TTR is present, where it drops from 5.2 pM in the arterial blood to 4.9 pM in *Liver* venous

blood (Fig. 9C). This is because *T3TTR* is the least abundant among the three T3-THBPs, thus

a large percentage drop is needed to meet the demand by *Liver tissue*. Interestingly, just like

the concentration gradients of *Total T4* and *Total T3* when all three THBPs are present, the

concentration gradients of *T4TBG* and *T3TBG*, *T4TTR* and *T3TTR*, or *T4ALB* and *T3ALB*

(which are essentially the total T4 and T3 respectively since only a single THBP species is

present in each case) are also basically linear and exhibit the same absolute drop (e.g., about

40 pM for T4 and 4.5 pM for T3 from segment 0 to segment 200 in *Liver blood*). These results

indicate that any of the three THBPs is sufficient to ensure uniform delivery of THs in tissues.

Lastly, we examined the situation when only one THBP is absent. With a combination of

any two THBPs present, the concentration gradients of *Total T4* and *Total T3* are also basically

linear and exhibit the same absolute drops as when all three THBPs are present, indicative of

uniform delivery of THs in tissues (Figs. S2-S4). *fT4* and the T4-THBP species that has the

shorter residence time for T4 always exhibit concave-upward decay profiles, while the T4-THBP

species that has the longer residence time exhibits a concave-downward decay profile. The

combination of ALB and TBG produces the most contrasted profiles (Fig. S3).

2.4 Heterogeneous transport and metabolism across tissue segments

The above spatial analysis has the underlying assumption that each of the cross-membrane

transport and metabolism parameters remains constant across the tissue segments from the

arterial to venous ends. However, this assumption may not be true for all tissues or organs. For

instance, the liver is known for its zonal heterogeneity in gene expression (Gebhardt and Matz-

Soja 2014). Thus, transporters such as MCT10 as well as TH-metabolizing enzymes such as

DIO1, UGT and SULT might have possible gradients from the periportal to central vein layers

within the liver lobule (Halpern et al. 2017). In this section, we explored how such intra-tissue

heterogeneity alters THBP contribution to TH tissue delivery and TH tissue concentrations. For

simplicity, a 10-fold linear gradient (either increasing or decreasing) was applied to one

parameter (k_{21}, $k_{23} - k_{35}$) at a time with the average equal to the default value used in the

homogenous case above. Below we reported the results for a select few parameters for the

Liver and the results for the remaining parameters are provided in Supplemental Material.

When k_{25}, the rate constant for T4 liver influx, increases from segment 1 through 200 (Fig. 11A), fT4 in *Liver blood* barely drops percentage-wise, exhibiting a small concave-down gradient (Fig. 11B, red line) as compared with the concave-up gradient when k_{25} is constant (Fig. 11B, gray line). *Total T4* in *Liver blood* decreases with a concave-down gradient vs. a linear gradient with constant k_{25}, but by the same amount in both cases (Fig. 11C). As far as T4 contributions by THBPs are concerned, they are all spatially dependent, but their nonlinearities are modulated by k_{25} variation as compared with constant k_{25} (Fig. 11E vs. Fig. 4A). ALB remains as the highest contributor throughout most segments, while TBG and TTR have similar contributions. The total amount of T4 unloaded by all three THBPs combined increases linearly across the segments. Correspondingly, T4 in *Liver tissue* increases linearly as well, by nearly 10-fold (Fig. 11D). The kinetic changes of T4 caused by the k_{25} gradient also affect T3. *fT3* in *Liver blood* exhibits a small nonmonotonic profile (Fig. 11G) and *Total T3* also has a U-shaped profile vs. a linear one with constant k_{25}, but it drops by the same amount in both cases (Fig. 11H). TBG still contributes to T3 the highest throughout most segments particularly downstream ones followed by ALB, and interestingly both revert to net loading of T3 toward the venous end (Fig. 11J). The total amount of T3 unloaded by all three THBPs combined decreases linearly across the segments. Despite that T4 in *Liver tissue* increases by 10-fold across the segments, T3 in *Liver tissue* is insensitive to the change, increasing only by 3% (Fig. 11I). A decreasing k_{25} gradient has opposite effects compared with an increasing k_{25} gradient. When k_{30}, the rate constant for T4 liver efflux, varies from segment 1 through 200, it has an opposite effect to varying k_{25} (Fig. S5). It is worth noting that T4 in *Liver tissue* is sensitive but T3 in *Liver tissue* is insensitive to k_{30} changes, with highly hyperbolic-like gradients despite k_{30} varying linearly (Fig. S5D and S5I). This nonlinearity is explained in Fig. S5 legend.

When k_{27}, the rate constant for T3 liver influx, increases or decreases from segment 1 through 200 (Fig. 12A), the gradients of all T4-related variables are barely affected (Fig. S6).

With an increasing k_{27} gradient, T3 in *Liver blood* is loaded onto as opposed to unloaded from

the THBPs in the upstream quarter of the segments (Fig. 12B). Moving downstream, ALB

unloads more T3 than TBG does, but ultimately TBG contribution surpasses ALB contribution.

With a decreasing k_{27} gradient, ALB initially contributes more T3, while TBG contributes the

most T3 throughout the majority of the downstream segments, and all THBPs revert to net

loading of T3 toward the venous end (Fig. 12C). The total amount of T3 unloaded by all three

THBPs combined changes linearly across the segments (Fig. 12 B and 12C). As k_{27} varies, *fT3*

and *Total T3* in *Liver blood* exhibit nonmonotonic profiles but the percentage changes are

negligibly small (Fig. 12D-12E). T3 in *Liver tissue* is sensitive to k_{27} – i.e., as k_{27} increases or

decreases linearly 10-fold, T3 changes by nearly 10-fold in the same direction (Fig. 12F). When

k_{31}, the rate constant for T3 liver efflux, varies from segment 1 through 200, it has an opposite

effect to varying k_{27}, and produces a sensitive hyperbolic gradient of T3 in *Liver tissue* without

affecting T4-related variables (Fig. S7).

When k_{26}, the rate constant for T4-to-T3 conversion in *Liver tissue*, varies from segment

1 through 200 by 10-fold (Fig. 13A), the gradients of *fT4* and *Total T4* in *Liver blood* deviate

slightly from the case when k_{26} is constant (Fig. 13B-13C). When k_{26} increases, the gradient of

T4 in *Liver tissue* is steeper than when k_{26} is constant, but the percentage drop remains

negligible, only about -0.5% (Fig. 13D, red line). When k_{26} decreases, the gradient of T4 in *Liver*

tissue is reversed, which increases by about 2% (Fig. 13D, green line). The relative

contributions to T4 in *Liver blood* by THBPs are similar to the case when k_{26} is constant (Fig.

13E and 13F vs. Fig. 4A). *fT3* and *Total T3* in *Liver blood* exhibit U-shaped profiles (Fig. 13G-

13H). Despite that the liver T4-to-T3 conversion rate constant k_{26} varies by 10-fold across the

segments, T3 in *Liver tissue* is insensitive to the changes, increasing or decreasing only by

about 3% (Fig. 13I). The changes in the relative contributions of THBPs to T3 unloaded in *Liver*

blood are similar to the case of varying k_{25} (Fig. 13J and 13K). Varying k_{34}, the rate constant for

T4 metabolism in *Liver tissue*, has a small effect on T4 gradient in *Liver tissue*, which only

changes by slightly > 1% from the arterial to venous ends, and the effect on T3 in *Liver tissue* is

negligible (Fig. S8). Varying k_{35}, the rate constant for T3 metabolism in *Liver tissue*, has no

effect on T4-related variables, and only causes a T3 gradient in *Liver tissue* that varies by < 6%

from the arterial to venous ends (Fig. S9).

Simulations were also conducted for *RB*-related parameters k_{21}, k_{28}, k_{23}, k_{29}, k_{24}, k_{32}, and

k_{33} respectively (Figs. S10-S16). In general, when compared to their counterparts in *Liver*,

applying gradients to these parameters modulates the THBP contributions to T4 and T3 tissue

delivery in a qualitatively similar fashion. Compared to the corresponding parameters in *Liver*,

however, T3 in *RB tissue* is much more sensitive to the gradients of k_{21}, k_{24}, k_{28}, k_{32}, and k_{33}, but

less sensitive to the gradients of k_{23} and k_{29}. T4 in *RB tissue* is still largely insensitive to the

gradients of most parameters except k_{21} and k_{28}.

Discussion

1. Contribution of THBPs to TH tissue delivery

1.1 Uniform TH tissue delivery

One of the most prominent functions of THBPs is to transport THs from the thyroid gland through the blood circulation to various target tissues and ensure uniform delivery of THs within the tissue where necessary as the blood perfuses. Our PBK models show minimal drops between the arterial and venous concentrations of free THs (Tables 1 and 2), suggesting that the cells at the vascular entrance of the tissues are exposed to nearly identical TH concentrations as those at the exit. The spatial model further demonstrates that nearly constant amounts of THs are unloaded in the first through the last tissue blood segments when no parameter gradients exist. Removing all three THBPs results in markedly steep concentration gradients of *fT4* and *fT3* as well as tissue T4 and T3, which is consistent with what was observed experimentally using *ex vivo* liver perfusion (Weisiger et al. 1986, Mendel et al. 1987, Mendel et al. 1988), and confirms the obligatory role of THBPs in maintaining uniform TH tissue delivery. However, the three THBPs are redundant and thus cross-compensatory in this role, as either one alone appears to be sufficient to maintain relatively constant TH concentrations through tissues. The sufficiency of ALB alone was previously demonstrated experimentally by using *ex vivo* liver perfusion (Mendel et al. 1987). It was further shown that T4 uptake in the liver, kidney and brain of Nagase analbuminemic rats was not different from normal rats (Mendel et al. 1989). TTR knockout mice are euthyroid with normal circulating free T4, T3, and TSH concentrations although total T4 and T3 are lower as expected (Palha et al. 1994). TBG-deficient patients have similar TH profiles and are also euthyroid (Mimoto and Refetoff 2020). Our results are consistent with these studies in that not all three THBPs specie are needed to maintain normal free TH concentrations and tissue uptake.

1.2 Contribution of individual THBP species

It has been argued that ALB supplies the most THs to tissues due to the shortest residence time

of THs on ALB; in contrast a smaller fraction of THs is supplied by TBG since THs have much

longer residence time on TBG (Mendel 1989, Schussler 2000). It has also been proposed that

TTR makes the most contribution to immediate T4 tissue delivery because of its Goldilocks

properties – it has the intermediate binding affinity for T4 and the abundance of T4TTR is

intermediate among the three T4-THBPs (Robbins 2002, Richardson 2009, Alshehri et al.

2015). The roles of TTR and TBG were also compared analogously to bank accounts, where

TTR is the checking and TBG the saving accounts such that T4TTR is tapped first for T4 tissue

delivery and then it is replenished by T4TBG later on after they leave the tissue (Robbins 2002,

Richardson 2009, Hamers et al. 2020). However, our models suggest neither of the two

hypotheses on the roles of ALB and TTR relative to TBG is valid.

Simulations of both the nonspatial and spatial models indicate that TBG, TTR and ALB

contribute comparable amounts of T4 in *Liver*, but TBG plays a dominant role in *RB* (Fig. 2 and

Tables 1 and 2). This is because the amounts of T4 unloaded by T4-THBPs are determined by

both their abundances and T4 residence time relative to the blood tissue transit time. TBG binds

the most T4 (75%) out of the three THBPs, which compensates for the longer residence time

and thus slower release of T4. The longer blood transit time in *RB* provides more time for TBG

to unload T4, which explains the much higher contribution of TBG to tissue T4 in *RB* than in

Liver. Therefore, for slowly perfused tissues, the contribution to tissue T4 follows the order of

the abundances of T4-THBPs. The residence time of T3 on THBPs are generally much shorter

than T4, especially for T3TBG and T3TTR, therefore the unloaded amounts are more aligned

with their relative abundance rather than the residence time. This explains the consistent order

of contribution to T3 by THBPs in both tissue compartments (Fig. 2), where TBG contributes

about 3 times more than ALB, and ALB nearly 4 times more than TTR.

Generally, for tissue uptake of a substance bound to plasma proteins, the dissociation

rate, rate of transportation or diffusion into the tissues, and blood perfusion rate can all play

some limiting roles depending on the parameter conditions (Weisiger 1985). The dissociation of

THs from a THBP species could be rate-limiting in providing THs for tissue uptake, the

significance of which depends on the tissue blood perfusion rate. For very slowly perfused

tissues, the THBP contribution to tissue TH follows the order and proportion of the abundances

of the TH-THBPs. In contrast, for rapidly perfused tissues, the percentage contribution by ALB

will become higher while that by TBG will become lower since the instantaneous T4 release

matters more. Ultimately it is the absolute dissociation rate, which is determined by both the TH

residence time on THBP and the abundance of TH-THBP, that dictates the amount of TH

released in the most rapidly perfused tissues.

In extremely rapidly perfused extrathyroidal tissues, it is conceivable that ALB is the

most liquid checking account, from which the vast majority of T4 and T3 are withdrawn and

delivered to the tissue. As the blood goes through the thyroid, ALB is quickly loaded with nearly

half of the newly synthesized T4, while TBG and TTR are loaded with the remaining half (Fig.

2A, Tables 1 and 2). Then as the thyroid venous blood mixes with the venous blood coming

back from other tissues, T4 will be transferred from ALB to TBG and TTR, as demonstrated by

the positive or negative sign of the difference between the association and dissociation rates for

each TH/THBP pair in *Body Blood* (Table S1). For T3, because of the relatively faster binding

kinetics and lower binding affinities between T3 and THBPs compared with T4, TBG seems to

be the THBP that is loaded with the most T3 in *Thyroid blood* (Fig. 2B, Tables 1 and 2).

Interestingly, after mixing with the venous blood coming back from other tissues in *Body Blood*,

both ALB and TTR transfer T3 to TBG (Table S1).

If T4TBG is too slow to release enough T4, it begs the question why TBG alone is

sufficient to unload a similar amount of T4 in *Liver* and *RB* as when all three THBPs are present

(Figs. 8 vs. 3). This is because with TBG alone, if *T4TBG* does not unload enough T4 in the

tissue, *T4TBG* in the venous blood would leave the tissue at a higher concentration than it

would be when T4 is sufficiently unloaded. After perfusing through the thyroid, *T4TBG* will be

recharged by the secreted T4 to an even higher level. With *T4TBG* in the arterial blood coming

back at a higher level to the tissue, the dissociation rate will be higher, thus more T4 is

unloaded. The slightly higher arterial *T4TBG* concentration is evidenced by the levels shown for

segment 0 in Fig. 8 compared with Fig. 3. In addition, because of the difference in residence

time, a larger drop of free THs in the first segment occurs when TBG is the only THBP (Fig. 8A

and 8C), which contrasts with the smaller drop of free THs when ALB is the only THBP (Fig.

10A and 10C). The initial larger drop in free THs moves TH-TBG further away from equilibrium,

reducing the association rate and allowing sufficient amounts of THs to be released from TH-

TBG.

1.3 Spatially dependent variation of THBP contribution

An interesting and novel finding of the present study is that the three THBPs unload THs in a

spatially dependent manner, where ALB generally contributes the most at the beginning

whereas TBG contributes the most at the end of the perfused tissue. This is due to different

residence times among the THBPs relative to the tissue blood transit time and different

abundances of TH-THBPs. At the beginning of tissue perfusion, there is not enough time for

THs to dissociate from TBG or TTR due to their longer residence time. As a result, ALB, which

has a shorter residence time, will unload more. The relative contribution of the THBPs to tissue

THs in the most upstream segments thus follows the order of the absolute dissociation rates of

each TH-THBP (Figs. 5 and 6). As the blood continues to move through the tissue with free THs

dropping, TBG and TTG will become further removed from their equilibrium, resulting in a higher

differential between the dissociation rate and association rate, thus more THs are unloaded

from TBG and TTR. Therefore, with longer perfusion time, the TH contribution by TBG and TTR

will catch up, while that by ALB will lessen. If the perfusion time is long enough, like in *RB* for

T3, the distances from equilibrium for the three THBPs will approach some constants (Fig. 6D-

6F), and the relative contribution by these three TH-THBPs will reach a fixed ratio proportional

to their abundances (Fig. 4D). At such a state, TBG is the one that is mostly removed from

equilibrium, while ALB is closest to equilibrium, with TTR in the middle. Being the furthest

removed from equilibrium allows TBG to deliver the most TH despite its tight grip on T4 and T3.

The spatially dependent, nonlinear kinetics of THBPs may explain some of the discrepancies in

the overall amounts of unloaded THs predicted by the spatial vs. nonspatial models. For

instance, the spatial model predicts that T4ALB unloads a slightly higher amount of T4 than

T4TBG does in *Liver* (Fig. 2A and Table 2), while the nonspatial model predicts the opposite

(Table 1). Such discrepancy underscores the importance of modeling tissue blood flow in

greater details for more accurate predictions.

The above conclusions are based on simulations with the assumption that the influx,

efflux, and metabolism parameter values are constant across the tissue segments. Our

simulations with spatial parameter heterogeneities indicate that they tend to modulate the

contributions of different THBP species to TH tissue delivery and may ultimately impact the

intra-tissue concentrations of T4 and T3 in some cases. Because of the near-equilibrium

kinetics of TH influx and efflux between the blood and tissues, especially for T4 in *Liver* and *RB*

and for T3 in *Liver* (Bagga et al. 2023), the intra-tissue T4 and T3 concentrations are mostly

sensitive to gradients of the respective influx and efflux parameters. In contrast, they are almost

insensitive to gradients of metabolism parameters except for T3 in *RB*. In the latter case, 10-fold

spatial variations of the metabolism parameters, such as T4-to-T3 conversion and elimination of

T4 and T3, can lead up to 1.66-fold changes in T3 in *RB tissue*. An implication of these results

is that for regulating local T3, varying DIO2 and DIO3 may not be sufficient in some cases, and

the membrane transporters may also need to be regulated. However, cautions should be

exercised when extrapolating to specific tissues as the *RB* here represents the average of all

extra-hepatic tissues. In tissues that do not operate in equilibrium mode, i.e., the influx and

efflux rates are considerably different, it is expected that local intracellular T3 would be more

sensitively regulated by variations in DIO2 and DIO3 than we predicted here. It is also well

known that multiple local feedback and feedforward mechanisms mediated by DIOs operate to

regulate tissue T3 homeostasis (Toyoda et al. 1995, Hosoi et al. 1999, Gereben et al. 2000,

Sagar et al. 2007, Rastogi et al. 2018). Therefore, the extent to which a tissue operates in the

equilibrium mode and the strength of local feedback/feedforward regulation may coordinately

control local T3 concentrations, depending on the developmental stages and tissues.

One example is how T3 determines the retina pattern formation during development. In

mice, T3 concentration forms a roughly 2.5-fold dorsal-to-ventral decreasing gradient in the

nascent retina on postnatal day 10 (Roberts et al. 2006). This gradient drives the formation of a

pattern where the medium-wavelength opsin expressing cone cells dominate in the dorsal retina

while the short-wavelength opsin expressing cone cells dominate in the ventral retina. The T3

gradient was not due to variations of DIO expression because DIO1 and 2 levels were

undetectable while DIO3 displayed a uniform distribution in the developing retina. It was argued

that graded TH transporter expression may create the T3 gradient in the retina, which is

consistent with our findings that intra-tissue T3 distribution is sensitive to influx and efflux

parameter gradients. In comparison, during metamorphosis of the frog, there is a DIO3 gradient

concentrated in the dorsal half of the developing retina, which leads to T3 accumulation in the

ventral half that drives the proliferation of ventral ciliary marginal zone (CMZ) cells and the

formation of the ipsilateral projection (Marsh-Armstrong et al. 1999).

The liver lobule is known for its zonal heterogeneity in gene expression (Gebhardt and

Matz-Soja 2014, Halpern et al. 2017). To meet different functional demands for THs in different

zones, there may exist spatial gradients of transporters and enzymes in their abundance and

affinity such that the rates of local influx, efflux, and metabolism of THs, and consequently,

hepatic TH concentrations may vary across zones. Based on our analysis, even if there are

gradients in the abundance and/or activities of the metabolic enzymes, but no gradients for the

transporters, T4 and T3 are not expected to form tangible gradients within the liver lobule. By

perfusing the rat liver through the portal vein with human serum containing ^{125}I-labeled T4, it

was shown that the hepatic T4 uptakes were similar in the different layers of the rat liver lobule

(Mendel et al. 1987), suggesting that there is no heterogeneous distribution of T4 transporters.

Antegrade and retrograde liver perfusions in the absence of THBPs further corroborated that the

periportal-to-central capacities for T4 uptake are relatively constant, at least in rat livers

(Weisiger et al. 1986, Mendel et al. 1988).

2. Evolutionary perspective on THBPs and their biological functions

Power et al., reviewed a wide array of studies on primitive vertebrates including fish,

amphibians, reptiles, and birds, suggesting that ALB emerged earlier than TTR evolutionarily

(Power et al. 2000). Since ALB binds many compounds weakly, it is not surprising that more

TH-specific THBPs arose as the organisms evolved. TBG appeared the latest with mammals

being the only animal class that have all three THBPs (McLean et al. 2017). Interestingly, these

THBPs share some homologous sequences in the domains involved in TH binding, especially a

5-residue TH-binding motif, with TH-binding apolipoproteins, cell membrane TH transporters,

and TH receptors, suggesting the origin of a common ancestor gene (Benvenga and Guarneri

2018).

Our PBK model indicates that efficient, uniform TH unloading in tissue blood can be

ensured even when only one of the three THBP species is present. It thus follows that the

THBPs that emerged later may have additional functions besides supplying THs to tissues. TTR

can be synthesized in the choroid plexus in the brain and placenta where it plays a unique role

in transporting THs against the local concentration gradients (Landers et al. 2013, Richardson et

al. 2015, Rabah et al. 2019). The late-emerging TBG appears to provide several additional

functions. T4 and T3 are predominantly associated with TBG in the plasma, and moreover,

among the three THBPs, TBG has the highest binding affinities for T4 and T3. Therefore, the

buffering function of THBPs against transient TH perturbations is mainly carried out by TBG.

Furthermore, the total amount of T4 in the plasma is equivalent to about 2-days' worth of T4

produced by the thyroid; therefore, THBPs, especially TBG, may function as an extrathyroidal

reservoir of THs, in addition to the intrathyroidal store in thyroglobulin, in the event of disruption

of TH production. TBG-deficient patients present with low total T4 and total T3 but have normal

concentrations of free THs and TSH and thus are euthyroid (Mimoto and Refetoff 2020). Our

simulations showed that in the absence of TBG the uniformity of TH unloading in tissues blood

is not affected, which is consistent with the lack of clinical manifestations in TBG-deficient

patients. The relative contribution of THBPs to tissue THs does not appear to be fixed and may

vary under different physiological and pathological conditions. For instance, TBG can be

regulated during acute inflammation, where locally released serine proteases can cleave TBG to

a low-binding-affinity form that can unload more THs to the inflammatory sites (Pemberton et al.

1988, Jirasakuldech et al. 2000). During pregnancy, the maternal TBG level steadily doubles

through the mid-term because of the rising estrogen and reduced plasma clearance, which may

function to titrate the increasingly produced maternal THs and prevent them from rising too high

(Moleti et al. 2014).

3. Limitations, potential applications, and future directions of the PBK models

Our current model does not include the HPT negative feedback loop. This is because we are

studying the local intra-tissue TH and THBP kinetics at steady state with constant inputs of

these species from the arterial blood. Therefore, it is not necessary to consider any actions of

THs on TSH and vice versa, the inclusion of which in the model is not expected to change the

results and conclusions in the present study. The uncertainty in the amounts of THs unloaded in

the tissue blood by each THBP species predicted by our models lies in the values reported in

the literature for the relative abundance of TH-THBPs and dissociation rate constants, which

can vary depending on individuals and their physiological conditions as well as the experimental

methodologies. The fraction of T4TBG may be overstated when measured with zone

electrophoresis by as much as more than 10% because of the comigration of T4-binding high-

density lipoprotein (HDL) and some Serpin proteins with TBG (Benvenga et al. 2002). Despite

such overestimation, the abundance of T4TBG is still expected to be much higher than T4TTR

and T4ALB; therefore, for slowly perfused tissues, the order of contribution to T4 by each THBP

species would remain largely unchanged because it primarily scales with the abundance of

each TH-THBP species. In contrast, the predicted relative contribution by each THBP species

for liver, a rapidly perfused tissue, is more uncertain because both the abundances and

dissociation rate constants of THBPs play a role here, but fewer experiments have been done to

determine the latter parameters.

While the three THBPs modeled here play major roles in regulating the amounts of THs

unloaded and thus available for tissue uptake, previous research indicated that lipoproteins

including HDL and low-density lipoprotein (LDL) also affect TH influx into and efflux out of cells

(Benvenga and Robbins 1990, Benvenga and Robbins 1998). In static cultures of skin

fibroblasts or hepatocytes, the net efflux of T4 out of the cultured cells was facilitated by the

lipoproteins as well as by THBPs (Benvenga and Robbins 1998). The facilitation can be partially

explained by these proteins acting as a sink to lower free T4 in the medium to reduce re-entry.

As a matter of fact, as long as the free fraction of T4 was titrated to the same level, regardless

of using either TBG, TTR, or ALB in the cell culture, T4 influx or uptake by the cells was reduced

to a similar magnitude (Benvenga and Robbins 1990). On an equal molar basis, the order of

efflux facilitation was TBG > LDL > TTR > HDL >> ALB, which cannot be explained by the

relative binding affinities of these proteins for T4 because lipoproteins are generally weaker T4

binders. It was postulated that LDL and HDL may engage some nonspecific physical contact

with the plasma membrane and their hydrophobic nature helps to desorb T4 off of the plasma

membrane. LDL is better than HDL in facilitating the efflux because of its higher lipophilic

content. Counterintuitively, it was also shown that LDL may facilitate T4 uptake (Benvenga and

Robbins 1990). This occurs in cells expressing LDL receptor (LDLR) (Benvenga and Robbins

1990), where after T4-carrying LDL docks to LDLR, T4 can be released and internalized by

cells. Such LDLR-mediated T4 entry may play a role in regulating lipid metabolism in local

tissues. Future iterations of our model may consider including LDL and HDL-mediated TH tissue

uptake.

The liver is an organ that can take up and secrete fatty acids, which can compete with

THs for ALB binding. Serum fatty acid concentrations can fluctuate as the blood transits through

different segments of the liver tissue when they are taken up from or secreted into the blood.

Thus, theoretically it is possible that such fluctuations may impact the local TH binding to ALB

and affect the spatial model accuracy. But the impact is unlikely to be significant, because at

physiological concentrations, THs only occupy a tiny fraction (about 0.0016%) of the binding

sites on ALB (Schussler 2000), so there are likely plenty sites available for fatty acids and other

molecules such as steroid hormones without tangibly displacing THs from ALB. Moreover,

experimental studies demonstrated that when myristate, a fatty acid that can bind to ALB with

high affinity (Fujiwara and Amisaki 2008), is present at concentrations 30-fold greater than

physiological levels, human serum ALB still retains a high-affinity binding site for T4 (the affinity

was only reduced by half), due to some conformational changes of ALB (Petitpas et al. 2003).

The intracellular distribution of THs can be heterogeneous as well. For instance, the nucleus

tends to accumulate much higher free T3 than the cytosol (Oppenheimer and Schwartz 1985).

Future iterations of the model may consider further compartmentalizing a tissue into cytosolic

and nuclear spaces if needed. Future updates to the model could also include splitting the *RB*

into separate tissue compartments as sufficient tissue-specific data such as TH tissue

concentrations, transporter and TH-metabolizing enzyme related kinetic parameters become

available.

For simplicity, we used a linear gradient and varied one parameter at a time to examine

their impact on THBP contributions to TH tissue delivery and tissue TH concentrations. In

reality, the gradients of transporters and metabolic enzymes can vary in shape which could be

exponential, nonmonotonic, or others. Moreover, the gradients of THs may not be controlled by

a single protein or enzyme. Rather, their gradients may multiplex to collectively regulate local

TH distributions within a tissue. As more tissue-specific spatial information becomes available,

they can be included in future models.

Our models and their future iterations can have several potential applications. It is well

known that the thyroid system is subjected to circadian regulation. In humans there are strong

daily rhythms of TSH and fT3 accompanied with less pronounced rhythm of fT4 (Nimalasuriya et

al. 1986, Russell et al. 2008). A strong temporal relationship between TSH and fT3 has been

suggested to associate with familial longevity (Jansen et al. 2015). Since THBPs carry THs in

blood circulations, they may affect the relative timing of TH tissue distribution. Applying control

theory, we are currently using the PBK model to study the amplitude and phase relationships

between TSH, fT3, fT4 and tissue THs and the potential mechanisms underpinning the

circadian patterns. Our model may also help with clinical chronotherapy to guide the timing of

dosing of thyroid drugs to ensure that the fluctuations of plasma THs are more closely aligned

with the natural circadian rhythm. Many environmental chemicals can interfere with TH binding

to THBPs because of their similar structures to THs. These endocrine-disrupting chemicals

(EDCs) include polychlorinated biphenyls (PCBs), dibenzo-p-dioxins, dibenzofurans, and

brominated flame retardants (Cheek et al. 1999, Hamers et al. 2006). EDCs, especially those

with high binding affinities, can displace THs from THBPs to cause a potential increase in fT4 or

fT3 levels (Brouwer et al. 1998, Noyes et al. 2019). Using the nonspatial version of the PBK

model, we have recently predicted that for persistent exposure to these EDCs the impact on

free THs is minimal, whereas daily intermittent exposure to EDCs with short half-lives may

cause concern as free THs can fluctuate to an extent that interferes with the circadian rhythm

(Bagga et al. 2023). The spatial model can be used to further investigate the impacts of thyroid

EDCs on tissue TH delivery by THBPs.

784   **Conclusion**

785   In summary, we have constructed a spatial PBK model with explicit considerations of TH and

786   THBP interactions and explored their differential contributions in supplying TH to tissues. While

787   it remains to be experimentally validated, the model provides novel insights into the debated

788   roles of THBPs in this regard and local TH regulations.

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794   **Conflict of Interest**

795   The authors declare no conflict of interest.

797   **Author Contributions**

798   QZ conceived the model structure, ADB constructed and simulated the model in MATLAB, ADB

799   and QZ conducted the parameter justification and estimation, and formal analysis of simulation

800   results, ADB and QZ wrote the initial draft and revised the manuscript. BPJ critically reviewed

801   and revised the manuscript.

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1008

 Figure Legend

Figure 1. Schematic illustrations of the human PBK model for T4 and T3. (A) The overall

structure of the PBK model (Bagga et al. 2023). *RB*: rest-of-body. QC: cardiac output (plasma

portion); QT, QRB, and QL: rate of blood (plasma) flow to *Thyroid*, *RB*, and *Liver* respectively;

CA: arterial concentration of a TH species; CVT, CVRB, and CVL: venous concentration of a TH

species in *Thyroid*, *RB*, and *Liver* respectively; $k_{20} - k_{35}$: rate constants for production, transport,

or metabolism processes as indicated. **(B)** Reversible binding of T4 and T3 with TBG, TTR and

ALB. These binding events occur in the plasma of all blood (sub)compartments/subsegments. k_1

$- k_{12}$: rate constants for association and dissociation between THs and THBPs as indicated.

Refer to (Bagga et al. 2023) for definitions and values of these parameters in (A) and (B). **(C)**

Illustration of tissue segmentation in the spatial PBK model. The tissue influx, efflux, T4-to-T3

conversion, and metabolism occur in all segments, but are only illustrated in the 1st segment.

1021

1022 **Figure 2. Percentage contributions of THBPs to loading and unloading of T4 (A) and T3**

1023 **(B) in tissue blood in the spatial PBK model.** Percentage contributions by ALB, TTR, and

1024 TBG in *RB*, *Liver*, and *Thyroid* compartments are indicated. Negative values denote TH

1025 unloading from THBPs and positive values denote TH loading to THBPs.

1026

Figure 3. Concentration gradients of free THs, TH-THBPs, and total THs in tissue blood in

the spatial PBK model. (A-E) Plasma concentrations of *fT4*, *T4TBG*, *T4TTR*, *T4ALB*, and *Total*

T4 in *Liver blood* (orange) and *RB blood* (green) respectively. **(F-J)** Plasma concentrations of

fT3, *T3TBG*, *T3TTR*, *T3ALB*, and *Total T3* in *Liver blood* (orange) and *RB blood* (green)

respectively. Concentrations in segment 0 represent the arterial concentrations and the

concentrations in segment 200 represent the venous concentrations.

1033

Figure 4. Segment-to-segment net differences in concentrations of free THs, TH-THBPs,

and total THs in tissue blood in the spatial PBK model. The value of concentration drop for

each segment is calculated by subtracting the concentration in the current segment from that in

the immediate upstream segment. For the drop in the first segment, the arterial blood

concentration (segment 0) is used as the upstream concentration. **(A-B)** Segment-to-segment

drops in plasma concentrations of *fT4*, *T4TBG*, *T4TTR*, *T4ALB*, and *Total T4*, as indicated in

(A), in *Liver blood* and *RB blood* respectively. **(C-D)** Segment-to-segment drops in plasma

concentrations of *fT3*, *T3TBG*, *T3TTR*, *T3ALB*, and *Total T3*, as indicated in (C), in *Liver blood*

and *RB blood* respectively.

1043

Figure 5. Evolution of the binding kinetics between T4 and THBPs through tissue blood

in the spatial PBK model. *Association rate* (solid blue), *Dissociation rate* (solid green), and

Distance from equilibrium (dashed orange) for *fT4* binding to *TBG* **(A)**, *TTR* **(B)**, and *ALB* **(C)** in

Liver blood. *Association rate*, *Dissociation rate*, and *Distance from equilibrium* for *fT4* binding to

TBG **(D)**, *TTR* **(E)**, and *ALB* **(F)** in *RB blood*. *Distance from equilibrium* = (*Dissociation rate -*

Association rate) */ Association rate* × 100%. Segment 0 represents the arterial blood. The same

color scheme is used for all panels as indicated in (A).

1051

Figure 6. Evolution of the binding kinetics between T3 and THBPs through tissue blood

in the spatial PBK model. *Association rate* (solid blue), *Dissociation rate* (solid green), and

Distance from equilibrium (dashed orange) for *fT3* binding to *TBG* **(A)**, *TTR* **(B)**, and *ALB* **(C)** in

Liver blood. *Association rate*, *Dissociation rate*, and *Distance from equilibrium* for *fT3* binding to

TBG **(D)**, *TTR* **(E)**, and *ALB* **(F)** in *RB blood*. *Distance from equilibrium* = (*Dissociation rate -*

Association rate) */ Association rate* × 100%. Segment 0 represents the arterial blood. The same

color scheme is used for all panels as indicated in (A).

1059

Figure 7. Concentration gradients of THs in blood and tissues in the absence all THBPs

in the spatial PBK model. (A-B) Plasma concentrations of *fT4* in *Liver blood* and *RB blood*

respectively. **(C-D)** Concentrations of T4 in *Liver tissue* and *RB tissue* respectively. **(E-F)**

Concentrations of *fT3* in *Liver blood* and *RB blood* respectively. **(G-H)** Concentrations of T3 in

Liver tissue and *RB tissue* respectively. Solid line: all THBPs absent, dashed line: all THBPs

present. Concentrations in segment 0 represent the plasma concentrations in arterial blood.

1066

1067 **Figure 8. Plasma concentration gradients of free THs and TH-TBGs in tissue blood with**

1068 **TBG as the only THBP present in the spatial PBK model. (A-B)** Plasma concentrations of

1069 *fT4* and *T4TBG* in *Liver blood* (orange) and *RB blood* (green) respectively. **(C-D)** Plasma

1070 concentrations of *fT3* and *T3TBG* in *Liver blood* (orange) and *RB blood* (green) respectively.

1071 Concentrations in segment 0 represent the plasma concentrations in arterial blood.

1072

1073 **Figure 9. Plasma concentration gradients of free THs and TH-TTRs in tissue blood with**

1074 **TTR as the only THBP present in the spatial PBK model. (A-B)** Plasma concentrations of

1075 *fT4* and *T4TTR* in *Liver blood* (orange) and *RB blood* (green) respectively. **(C-D)** Plasma

1076 concentrations of *fT3* and *T3TTR* in in *Liver blood* (orange) and *RB blood* (green) respectively.

1077 Concentrations in segment 0 represent the plasma concentrations in arterial blood.

1078

1079 **Figure 10. Plasma concentration gradients of free THs and TH-ALBs in tissue blood with**

1080 **ALB as the only THBP present in the spatial PBK model. (A-B)** Plasma concentrations of

1081 *fT4* and *T4ALB* in *Liver Blood* (orange) and *RB Blood* (green) respectively. **(C-D)** Plasma

1082 concentrations of *fT3* and *T3ALB* in *Liver blood* (orange) and *RB blood* (green) respectively.

1083 Concentrations in segment 0 represent the plasma concentrations in arterial blood.

1084

Figure 11. Effects of k_{25} gradients across *Liver* segments on TH concentrations in *Liver*
and contributions of THBPs to TH loading and unloading in the spatial PBK model. (A)
Linearly increasing, decreasing, or constant k_{25} gradients implemented as indicated. **(B-D)** T4
concentrations in *Liver blood* and *Liver tissue* as indicated. **(E-F)** Segment-to-segment net
differences in plasma concentrations of *fT4*, *T4TBG*, *T4TTR*, *T4ALB*, and *Total T4* as indicated
in *Liver blood* for increasing and decreasing k_{25} gradients respectively. **(G-I)** T3 concentrations
in *Liver blood* and *Liver tissue* as indicated. **(J-K)** Segment-to-segment net differences in
plasma concentrations of *fT3*, *T3TBG*, *T3TTR*, *T3ALB*, and *Total T3* as indicated in *Liver blood*
for increasing and decreasing k_{25} gradients respectively. The same color scheme is used for
panels (B-D, G-I) as indicated in (A), for panel (F) as in (E), and for panel (K) as in (J).

Figure 12. Effects of k_{27} gradients across *Liver* segments on T3 concentrations in *Liver*
and contributions of THBPs to T3 loading and unloading in the spatial PBK model. (A)
Linearly increasing, decreasing, or constant k_{27} gradients implemented as indicated. **(B-C)**
Segment-to-segment net differences in plasma concentrations of *fT3*, *T3TBG*, *T3TTR*, *T3ALB*,
and *Total T3* as indicated in *Liver blood* for increasing and decreasing k_{27} gradients
respectively. **(D-F)** T3 concentrations in *Liver blood* and *Liver tissue* as indicated. The same
color scheme is used for panels (D-F) as indicated in (A), and for panel (C) as in (B).

Figure 13. Effects of k_{26} gradients across *Liver* segments on TH concentrations in *Liver*
and contributions of THBPs to TH loading and unloading in the spatial PBK model. (A)
Linearly increasing, decreasing, or constant k_{26} gradients implemented as indicated. **(B-D)** T4
concentrations in *Liver blood* and *Liver tissue* as indicated. **(E-F)** Segment-to-segment net
differences in plasma concentrations of *fT4*, *T4TBG*, *T4TTR*, *T4ALB*, and *Total T4* as indicated
in *Liver blood* for increasing and decreasing k_{26} gradients respectively. **(G-I)** T3 concentrations
in *Liver blood* and *Liver tissue* as indicated. **(J-K)** Segment-to-segment net differences in

1111 plasma concentrations of *fT3*, *T3TBG*, *T3TTR*, *T3ALB*, and *Total T3* as indicated in *Liver blood*

1112 for increasing and decreasing k_{26} gradients respectively. The same color scheme is used for

1113 panels (B-D, G-I) as indicated in (A), for panel (F) as in (E), and for panel (K) as in (J).

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1116 **Tables**

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Table 1. Loading and unloading of THs in tissues by THBPs in nonspatial PBK model

		Free TH		TH-TBG		TH-TTR		TH-ALB	
		Conc (pM)	CV-CA (pM) / % change	Conc (pM)	CV-CA (pM) / % change	Conc (pM)	CV-CA (pM) / % change	Conc (pM)	CV-CA (pM) / % change
T4	CA	15.0019	na	7.0046E4	na	1.6003E4	na	7.2754E3	na
	$CV_{Thyroid}$	17.4036	+2.4017 / +16.01%	7.055E4	+504 / +0.7198%	1.6467E4	+463 / +2.895%	8.1783E3	+903 / +12.41%
	CV_{Liver}	14.9745	-0.0274 / -0.1824%	7.0031E4	-15.175 / -0.0217%	1.5992E4	-11.753 / -0.0734%	7.2631E3	-12.264 / -0.169%
	CV_{RB}	14.9901	-0.0117 / -0.0781%	7.0034E4	-11.782 / -0.0168%	1.5996E4	-7.496 / -0.0468%	7.2698E3	-5.592 / -0.077%
T3	CA	5.0089	na	1.2758E3	na	82.2077	na	331.36	na
	$CV_{Thyroid}$	5.9337	+0.9247 / +18.46%	1.3466E3	+70.8 / +5.55%	92.0188	+9.811 / +11.93%	383.59	+52.23 / +15.76%
	CV_{Liver}	4.9879	-0.021 / -0.4194%	1.2727E3	-3.0267 / -0.237%	81.9134	-0.2943 / -0.358%	330.04	-1.3206 / -0.3985%
	CV_{RB}	5.0045	-0.0044 / -0.0879%	1.275E3	-0.7841 / -0.0615%	82.1397	-0.0681 / -0.0828%	331.07	-0.2876 / -0.08679%

Note: na, not applicable. CA: arterial concentration, CV: venous concentration, % change = (CV-CA)/CA.

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Table 2. Loading and unloading of THs in tissues by THBPs in spatial PBK model

		Free TH		TH-TBG		TH-TTR		TH-ALB	
		Conc (pM)	CV-CA (pM) / % change	Conc (pM)	CV-CA (pM) / % change	Conc (pM)	CV-CA (pM) / % change	Conc (pM)	CV-CA (pM) / % change
T4	CA	14.9978	na	7.0033E4	na	1.5999E4	na	7.2734E3	na
	$CV_{Thyroid}$	17.3995	+2.4017 / +16.01%	7.0537E4	+504 / +0.72%	1.6462E4	+463 / +2.90%	8.1764E3	+903 / +12.41%
	CV_{Liver}	14.9671	-0.0307 / -0.20%	7.0020E4	-13.0744 / -0.0187%	1.5987E4	-11.7385 / -0.0734%	7.2590E3	-14.3806 / -0.1977%
	CV_{RB}	14.9853	-0.0125 / -0.084%	7.0022E4	-10.74 / -0.0153%	1.5991E4	-8.0595 / -0.0504%	7.2673E3	-6.0681 / -0.0834%
T3	CA	5.0047	na	1.2748E3	na	82.1376	na	331.077	na
	$CV_{Thyroid}$	5.9294	+0.9247 / +18.48%	1.3456E3	+70.8145 / +5.56%	91.9485	+9.8109 / +11.94%	383.303	+52.226 / +15.77%
	CV_{Liver}	4.9829	-0.0218 / -0.44%	1.2718E3	-2.9384 / -0.2305%	81.8216	-0.3161 / -0.3848%	329.684	-1.3933 / -0.4208%
	CV_{RB}	5.0003	-0.0044 / -0.088%	1.2740E3	-0.7791 / -0.0611%	82.0688	-0.0688 / -0.0838%	330.787	-0.2896 / -0.0875%

Note: na, not applicable. CA: arterial concentration, CV: venous concentration, % change = (CV-CA)/CA.

Figure 1

A

B

C

Figure 2

A

% T4 unloaded or loaded by THBPs

B

% T3 unloaded or loaded by THBPs

Figure 3

Figure 4

Figure 5

Figure 6

Figure 7

Figure 8

Figure 9

Figure 10

Figure 11

Figure 12

Figure 13