Topographical polarity reveals continuous EEG microstate transitions and electric field direction in healthy aging

Shiho Kashihara[1], Tomohisa Asai[1], & Hiroshi Imamizu[1,2]

[1] Department of Cognitive Neuroscience, Cognitive Mechanisms Laboratories, Advanced Telecommunications Research Institute International (ATR), Keihanna Science City, Kyoto 619-0288, Japan.

[2] Department of Psychology, Graduate School of Humanities and Sociology and Faculty of Letters, The University of Tokyo, 7-3-1 Hongo, Bunkyo-ku, Tokyo 113-8654, Japan.

* Correspondence: Shiho Kashihara, Department of Cognitive Neuroscience, Cognitive Mechanisms Laboratories, Advanced Telecommunications Research Institute International (ATR), Keihanna Science City, Kyoto 619-0288, Japan. E-mail: skashihara@atr.jp

Abstract

EEG microstate sequences, representing whole-brain spatial potential distribution patterns of the EEG, offer valuable insights for capturing spatiotemporally continuous and fluctuating neural dynamics with high temporal resolution through appropriate discretization. Recent studies suggest that EEG microstate transitions are gradual and continuous phenomena, contrary to the classical view of binary transitions. This study aimed to update conventional microstate analysis to reflect continuous EEG dynamics and examine differences in age-related electrophysiological state transitions. We considered the relative positions of EEG microstates on the neural manifold and their topographical polarity. Transition probability results showed fewer transitions on the microstate D-C-E axis in older adults. In contrast, transitions among microstates A, D, and B increased in the older group and were mainly observed within polarity. Furthermore, the 100 microstate transitions, which are variations of the shortest transitions between 10 microstates, could be reduced to 8 principal components based on the co-occurrence of each transition, including hubs C and E, planar transitions through msA/B and D, and unidirectional transition components. Several transition components were potentially significant predictors of age group. These features were nearly replicated in independent data, indicating their robustness in characterizing age-related electrophysiological spatiotemporal dynamics.

Keywords: EEG microstates, aging, topographical polarity, state transition

Statements and Declarations

Funding: This work was supported by JST [Moonshot R&D][Grant Number JPMJMS2291], NICT [Research and development of technology for enhancing functional recovery of elderly and disabled people based on non-invasive brain imaging and robotic assistive devices], and the collaboration fund of XNef Inc. and Shionogi & Co., Ltd.

Conflict of interest: The authors declare that they have no conflict of interest.

Ethics approval: Study 2 was approved by the Ethical Committee of ATR (approved number: 19-144).

Availability of data and material: The data in Study 2 are available from the authors upon reasonable request.

Acknowledgments: We are grateful to Takamasa Hamamoto and Ayako Tsukamoto for their help with data collection in Study 2.

Authors' contributions: SK and TA contributed to the study's conception and design, material preparation, data collection, and analysis. SK wrote the first draft of the manuscript, and TA and HI commented on the manuscript. All authors read and approved the final manuscript.

1. **Introduction**

The resting brain is recognized for its structured activity, linked to various cognitive functions, mental states, and psychological characteristics. This activity demonstrates that the resting brain is neither inactive nor merely random in the absence of stimuli (Greicius, 2008; Gusnard et al., 2001; Miall & Robertson, 2006; Northoff et al., 2010; Stevens & Spreng, 2014). One of the most significant examples of the many aspects related to the resting brain is aging (Andrews-Hanna et al., 2007; Ferreira & Busatto, 2013; Hausman et al., 2020; Varangis et al., 2019). This paper focuses on discretizing the spatiotemporal dynamics of resting electroencephalography (EEG) using a newly developed methodology, with a focus on the effects of aging.

Accumulated studies have revealed that aging is accompanied by various changes in the brain (Aron et al., 2022; Cleeland et al., 2019; Li et al., 2001; Oschwald et al., 2019; Samson & Barnes, 2013). Not only age-related changes in brain structure (Good et al., 2001; Lebel et al., 2010; Oschwald et al., 2019; Resnick et al., 2003) and resting-state functional magnetic resonance imaging (fMRI) functional connectivity (Ferreira & Busatto, 2013; Ferreira et al., 2016; Geerligs et al., 2015; Sala-Llonch et al., 2015), but also age-related differences in the brain are manifested in the electrophysiological neural aspect. For example, research has repeatedly shown that the alpha band frequency activity in the resting-state EEG becomes slow, and its power decreases with age (Babiloni et al., 2006; Chiang et al., 2011; Ishii et al., 2017; Klimesch, 1999; Merkin et al., 2023; Scally et al., 2018; Tröndle et al., 2023).

Despite the growing body of research in cognitive neuroscience related to aging, the spatiotemporal dynamics of whole-brain states with aging remain unclear. EEG is a powerful tool for capturing temporal neural dynamics with good temporal resolution. However, most EEG studies have focused on time- and/or frequency-domain activity in local spatial areas and did not consider whole-brain dynamics. One method for capturing the global spatiotemporal dynamics of whole-brain EEG is EEG microstate analysis (Khanna et al., 2015; Michel & Koenig, 2018). EEG microstates are spatial patterns of scalp potential topographies that transition metastably within a time frame of approximately 40–120 milliseconds (Kleinert et al., 2024; Michel & Koenig, 2018). They reflect the large-scale neural dynamics of brain networks predominant in scalp EEG (Zanesco et al., 2020). Traditionally, four classical microstates have been defined: A, B, C, and D (Michel & Koenig, 2018). Additionally, several additional states are sometimes referred to: C', E, F, or G (Custo et al., 2014, 2017; Tarailis et al., 2021, 2024). The naming of state labels has diverged across studies due to independent definitions by researchers or naming based on visual similarity or similarity indices with labels reported in previous studies. However, some integration has been attempted recently (Tarailis et al., 2024). The relationship between microstates and function and state of mind continues to interest researchers (Britz et al., 2010; Khanna et al., 2015; Milz et al., 2016; Musso et al., 2010; Panda et al., 2016; Seitzman et al., 2017; Tarailis et al., 2024; Yuan et al., 2012).

Studies examining the relationship between EEG microstates and aging suggest that aging alters specific states, including microstates C, D, and E. In early studies, Koenig et al. (2002) and Tomescu et al. (2018) focused on developmental changes in microstates. They preliminarily described that the state duration of microstate C and the transition probability between microstates C and D decreased with age. It is worth noting that microstate D in Tomescu et al. (2018) appeared to be somewhat posterior-active and thus closer to microstate E, according to the relabeling procedure of Tarailis et al. (2024). Furthermore, a recent study by Zanesco et al. (2020) examined age differences in EEG microstate dynamics using a large open dataset. They found that older adults had larger global explained variances (GEVs) for

microstates A and B, smaller GEVs for microstates C and E, and longer average durations
and less occurrence in all microstate classes than younger adults. Furthermore, they also
suggested that transitions from one state to microstates A and B were more frequent in older
adults, while transitions from one state to microstate C and from C to E were fewer in older
adults (Zanesco et al., 2020). Additionally, Jabès et al. (2021) revealed that older people have
lower GEVs, occurrences, and transitions from one state to microstates C and C' (noting that
their C' can be relabeled to E; cf., Tarailis et al., 2024).

While findings on age-related microstates are emerging, conventional microstate
analysis methodologies have several limitations in providing an adequate discretized
representation of continuous EEG spatiotemporal dynamics. The first problem lies in that the
labeling of microstates ignores topographical polarity. Conventional microstate analysis has
ignored topographical polarity to focus on the electric field pattern in resting-state EEG
analysis (Michel & Koenig, 2018; Murray et al., 2008). This technique of ignoring polarity aids
in suppressing the impact of unstable and noisy electric fields associated with the inversion of
neuronal generators providing EEG oscillations and identifying the persistence of stable states
irrespective of the dominant frequency of EEG oscillation (Michel & Koenig, 2018). However,
it may not be ideal for characterizing the essentially continuous EEG dynamics in the
representation of broad-band spatiotemporal dynamics as a linear sum of activity over multiple
frequency bands. Changing topography can indicate changes in global network activity since
differences in the spatial representation of the potential map imply differently distributed
neuronal generators' activation (Khanna et al., 2015; Michel & Koenig, 2018). However, the
same topography does not imply the same neuronal generator activation. Such an interpretive
problem also applies to polarity-reversed topographical patterns. In other words, reversing
neuronal generators in the brain may produce polarity-reversal topographies, but this does not
mean that all polarity-reversal topographies originate from the same neural generators as the
immediately preceding topography. The polarity of the EEG depends on the structural
constraints of the brain (e.g., the orientation of the pyramidal cells), instrumental constraints
(e.g., electrode orientation and reference position), and changes in E/I balance as the balance
between excitatory and inhibitory neurotransmission, as well as the EEG oscillation
(Kirschstein & Köhling, 2009). Hence, it is reasonable to assume that polarity in EEG
topography has necessary information reflecting the composition of the whole-brain electric
field potentials. Therefore, fitting microstate labels to the data in consideration of topographical
polarity can aid in understanding the characteristics of EEG spatiotemporal dynamics.

The second problem is that previous microstate studies have relied primarily on static
indices. While several quantification indices for EEG microstates exist, the most commonly
used measures, such as duration (i.e., how many seconds a state lasts on average) and
occurrence (i.e., how often a state occurs on average per second), are static. They are
summaries of state characteristics, such as how often or how long a state appears during a
specific period, which do not reflect the spatiotemporal continuity of the EEG dynamics.
Moreover, these static indices are sensitive to the analysis software and parameters (e.g.,
temporal smoothing); thus, they can be unstable. Popov et al. (2023) examined the test-retest
reliability of various resting-state EEG indices in younger and older participants. They
highlighted the low test-retest reliability of EEG microstate measures, particularly among older
individuals. While the stability and reliability of EEG microstate indices remain subjects of
debate (Antonova et al., 2022; Khanna et al., 2014; Kleinert et al., 2024; Liu et al., 2020; Popov
et al., 2023; Zanesco et al., 2020), indices that focus on temporal transitions between states,
such as state transition matrices, might be informative, especially for describing continuous
trajectories.

Research findings suggest that EEG microstates and their inter-label transitions
appear to be continuous rather than discrete (Mishra et al., 2020; Shaw et al., 2019). Therefore,
microstate label sequences can be an effective continuative discretization method for
characterizing the originally continuous spatiotemporal EEG dynamics. Asai et al. (2023) have
shown that the dynamics of continuous EEG topographies can be visualized as continuous
trajectories on spherical neural manifolds defined based on dissimilarities between
topographies (see Figure S1).. In their methods, neural states are distributed on a closed
spherical surface based on the dissimilarity between states, and EEG microstates are
represented as attractors in the EEG state space (Férat et al., 2022; Milz et al., 2017). In this
context, describing EEG time series as transitions between microstate labels (e.g.,
AACCCDDDBCC…) can be compared to dividing a closed neural manifold ("the earth;"
spherical surface) into several areas ("countries;" arbitrary boundary) and then describing the
entry and leave history between countries ("immigration control"). Thus, examining EEG
microstate transition offers a suitable approach for discretizing the continuous spatiotemporal
dynamics of EEG. Importantly, since each neural state has a topographical polarity, labeling
that ignores this polarity leads to the "jumping" of states (Mishra et al., 2020), which cannot
account for the continuous trajectories on the spherical manifold. In other words, the two
problems of considering topographical polarity and focusing on state transitions are
interrelated; therefore, labeling EEG microstates by considering topographical polarity is
necessary to properly quantify spatiotemporally continuous dynamics by focusing on state
transitions.

In this study, we extended the EEG microstate approach by considering the
topographical polarity, especially from the viewpoint of state transitions. We examined the
differences in EEG discrete state transitions between younger and older participants. To begin,
utilizing a large open dataset (Babayan et al., 2019), we explored the characteristics of the
transition matrix between the younger and older adults when topographical polarity was
considered, checking for consistency with previous findings of fewer transitions to microstates
C and E in the older adults (Study 1). In addition to examining individual transition probabilities
between microstates, we attempted to represent coarse-grained EEG dynamics in terms of
units of "transition components," which were groups of similar transitions. This enabled us to
identify consistent effects regardless of the unit of measurement scale when examining the
relationship between neurodynamic and psychodynamic aspects such as aging. Furthermore,
utilizing independent data, we verified whether the transition characteristics between younger
and older adults identified in Study 1 could be reproduced at each index scale (Study 2). In
this paper, we used the term "positive (+)" topographical polarity, defined as a pattern in which
the overall potential of the frontal electrode population is positive and the occipital is negative,
and the opposite is termed "negative (-)" topographical polarity (cf., Asai et al., 2022).

2. Study 1 : Exploratory analysis of topographical polarity considerations using
an open dataset

Study 1 utilized the LEMON dataset (Babayan et al., 2019) to compare the transition
matrices of microstate label sequences between age groups by considering topographical
polarity. This large open dataset has been used in previous studies on EEG microstates
(Zanesco et al., 2020). Despite some differences from the study by Zanesco et al. (2020),
such as data exclusion criteria and the parameters of the preprocessing and microstate
analysis, we expected to replicate their findings that transitions to microstates C and E reduced

and transitions to microstates A and B increased in older adults. Moreover, we attempted to
extend Zanesco et al. (2020) and other previous studies by considering topographical polarity.
By describing microstate sequences considering topographical polarity, we could
quantify the transitions between EEG discrete categories while preserving the continuous
spatiotemporal dynamics, as expressed as trajectories on neural manifolds (Asai et al., 2023).
Previous studies have suggested that the temporal dynamics of EEG are slower and more
unitary in older people (e.g., lower peak frequency of oscillation [Ishii et al., 2017; Merkin et
al., 2023; Scally et al., 2018] and lower signal variability, i.e., higher regularity in a fundamental
dynamic system [Deery et al., 2023; Lau et al., 2022; Ma et al., 2021]). Therefore, the extended
microstate sequence used in the present study, which enables us to follow more detailed
transitions while accounting for topographical polarity, may emphasize differences in
spatiotemporal transition dynamics characteristic of younger and older adults. Hence, to
determine what differences in transition dynamics exist between younger and older adults, we
conducted an exploratory analysis without specific hypotheses regarding the differences in
transitions that account for topographical polarity.
212
2-1. Methods
2-1-1. Data description
We accessed an openly available, published dataset called LEMON (Babayan et al.,
2019), consisting of 227 adults categorized into two age groups: younger (20–35 years of age;
N = 153; female, n = 45; male, n = 108; mean age = 25.1 years, SD = 3.1) and older (59–77
years of age: N = 74; female, n =37; male, n = 37; mean age = 67.6 years, SD = 4.7) groups.
The large-scale study conducted by Babayan et al. (2019) involved questionnaires, interviews,
resting-state EEG and fMRI measurements, cognitive tasks, and other assessments over
several days. Data were collected by Babayan et al. (2019) as a part of the Max Plank Institute
Leipzig Mind-Brain-Body study database; according to Babayan et al. (2019), their study was
conducted in accordance with the Declaration of Helsinki and was approved by the ethics
committee at the medical faculty of the University of Leipzig (reference number 154/13-ff). The
open data they published were documented, curated, and made available for research
purposes (Babayan et al., 2019).
Our interest was in resting-state EEG data. The resting-state EEG was recorded for
16 minutes, consisting of eight consecutive blocks of 1 minute each of eye-closed and eye-
opened rest in interleaved order. A 62-channel (61 scalp electrodes according to the
international standard 10-10 system and one vertical EOG electrode below the right eye)
actiCAP and BrainAmp MR plus amplifier (Brain Products GmbH, Gilching, Germany) were
used for EEG recording, with a sampling rate of 2500 Hz. More details are available in
Babayan et al. (2019). We downloaded openly accessible raw data (N = 215), categorized into
younger (N = 144; female, n = 44; male, n = 100; estimated mean age = 22.9 years, SD = 3.4)
and older (N = 71; female, n = 35; male, n = 36; estimated mean age = 65.4 years, SD = 4.6)
groups. The LEMON dataset only provides participant ages as discretized 5-year bins for
anonymity. Therefore, the minimum value of the discretized bin was used to calculate the
estimated mean age and SD of each age group (cf., Zanesco et al., 2020). It is noteworthy
that for the 55–60 years age bin, all participants were considered 59 years old because the
age range for older participants was 59–77 years (Babayan et al., 2019).
241
242   2-1-2. Preprocessing of resting-state EEG data
243   After preprocessing, data from 25 participants (14 younger and 11 older participants)
244   were excluded for the following reasons: extremely small data sizes of the downloaded data

files compared to the others, 10 participants (3 younger and 7 older); lack of marker file, 1 younger participant; something wrong with triggers, 2 younger participants; and positive drug tests, 12 participants (8 younger and 4 older). Preprocessing was applied for the 16-minute continuous resting-state EEG data, which comprised a mixture of eye-closed and eye-opened blocks. Our preprocessing procedure is described below. All analyses were conducted using EEGLAB v2019.1 (Delorme & Makeig, 2004) under MATLAB R2019a (Mathworks Inc., Natick, MA, USA).

First, we downsampled data to 250 Hz and applied a Hamming windowed sinc finite impulse response (FIR) filter from 2 to 20 Hz using the EEGLAB function "*pop_eegfiltnew*" of the EEGLAB plugin "*firfilt* (v2.4)". We removed the vertical EOG channel and then conducted bad channel identification. We employed the artifact subspace reconstruction method (ASR: Mullen et al., 2015) with a threshold of 20 *SD* (Chang et al., 2018) using the EEGLAB function "*clean_artifact*" of the EEGLAB plugin "*clean_rawdata* (v2.3)." The criteria for detecting bad channels were as follows: flat signal longer than 5 seconds, line noise greater than 4 *SD* from the entire signal of that channel, and poor correlation with adjacent channels by less than 85%. These bad channels were removed and interpolated using the EEGLAB function "*pop_interp*." Under these criteria, an average of 2.62 (*SD* = 3.05, range = 0–16 channels) were detected as bad channels. In addition, ASR results showed that an average of 91.92% (*SD* = 6.40, range = 66.37–99.91%) of the original data were preserved, and the rest were reconstructed as containing non-stationary artifacts.

Subsequent to re-referencing the data to the average potential, adaptive mixture independent component analysis (Hsu et al., 2018; Palmer et al., 2011) was applied using the EEGLAB plugin "*AMICA* (v1.5.1)." Dipole estimation was also conducted using the EEGLAB functions "*dipfit* (v3.3)" and "*fitTwoDipoles* (v0.01)." We then calculated the probability of each of the seven source categories for each independent component (IC) using the ICLabel toolbox (Pion-Tonachini et al., 2019) within the EEGLAB plugin "*ICLabel* (v1.3)." Only ICs that met all three of the following criteria were retained as ICs reflecting the signal and returned to the electrode space for further analysis: ICs labeled "brain" by *ICLabel*, ICs with residual variance lower than 15% (Artoni et al., 2014), and ICs for which dipole was estimated in the brain. A mean of 28.40 ICs (*SD* = 6.71, range = 7–46 ICs) met these criteria.

After data cleaning, the data were divided into eye-opened and eye-closed blocks (one minute each, a total of eight blocks per condition). The eight eye-opened and eye-closed blocks were concatenated and treated as eight-minute resting data. Finally, a total of 190 datasets, including 130 in the younger group (female, *n* = 37; male, *n* = 93; estimated mean age = 22.8 years, *SD* = 3.3) and 60 in the older group (female, *n* = 30; male, *n* = 30; estimated mean age = 65.2 years, *SD* = 4.5) were used in subsequent analyses.

2-1-3. EEG microstate analysis

We conducted EEG microstate analysis using some of the functions of the EEGLAB plugin "*MST1.0*" (Poulsen et al., 2018). The microstate analysis consisted of two phases: a clustering phase to find dominant configuration maps using eye-closed resting data from all 190 participants and a template-matching phase in which the obtained templates were applied to the data of each participant to yield microstate label sequences. It should be noted that temporal smoothing was not applied during EEG microstate analysis in Studies 1 and 2, as our focus was on describing the natural state of continuous spatiotemporal dynamics.

We first calculated the global field power (GFP) time series to extract data for the clustering process. We identified the topography of the local GFP maxima (i.e., peak) for each participant's EEG time series. GFP is a reference-independent measure of response strength,

calculated as the standard deviation of all electrodes at a given time (Murray et al., 2008;
Poulsen et al., 2018). The GFP peak point is known to maximize the signal-to-noise ratio of
the topography and provide an optimal representation of quasi-stable spatial topographies
(Khanna et al., 2015; Mishra et al., 2020; Zanesco, 2020). Of the topographies at the GFP
peak points for each participant, 192 were randomly selected per participant for the younger
group and 417 topographies for the older group, with a constraint of a 10 ms minimum peak
interval. This weighting aimed to correct for the effect of the different number of participants in
the younger and older age groups on the microstate templates. It was set up to result in
approximately 50,000 data points for clustering, with equal contributions from both age groups
(i.e., [50,000 points/2 groups]/130 younger participants ≈ 192 points, and [50,000 points/2
groups]/60 older participants ≈ 417 points).

Subsequently, non-hierarchical clustering was performed on the extracted GFP peak
topographies (49,980 topographies in total) using the modified k-means method (Mishra et al.,
2020; Pascual-Marqui et al., 1995) (k = 2:8, 50 random initializations of algorithm, and 1,000
maximum iterations) using the "*pop_micro_segment*" function in the EEGLAB plugin "*MST1.0*"
(Poulsen et al., 2018). After that, we determined the optimal number of clusters based on the
cross-validation (CV) criterion (Murray et al., 2008; Pascual-Marqui et al., 1995). The resulting
microstate template maps corresponded to a unit-length basis vector defining a 1-D subspace
embedded in a k-dimensional space (Mishra et al., 2020). We aimed to incorporate
topographical polarity into the template-matching process for the EEG time series data maps.
To achieve this, we opted to use twice the optimal number of k maps obtained using the
modified k-means algorithm. This encompassed both the original maps and their inverted
counterparts, resulting in a total of k*2 microstate templates used in this study.

Next, the template maps were matched to the original EEG recordings for each
participant to yield a time series sequence of microstates using the "*pop_micro_fit*" function in
the EEGLAB plugin "*MST1.0*" (Poulsen et al., 2018). For all sampling points comprising each
participant's eye-closed resting-state EEG time series, the spatial correlations between the
template maps and the topography map of each sampling point were calculated. Subsequently,
the topographical map of each point was classified into template labels that showed the
highest spatial correlation ("winner-take-all"). Importantly, when considering topographical
polarity, the assignment of template labels involved referencing a template map that included
both the original map and its polarity-reversed counterpart. In addition, no temporal smoothing
was applied.

The obtained microstate label sequences were divided into transitions between two
consecutive states using sliding windows of two-time points with 50% overlap. The number of
transitions was counted for a total of 100 transitions: the combination of [optimal number of
k×2] previous states ("from" state) × [optimal number of k×2] following states ("to" state).

In terms of comparing age differences for each transition pair, we defined a transition
probability matrix as follows: the transition probability matrix was calculated by averaging the
transition probability matrix of each individual obtained by first counting the number of
microstate label transitions between two consecutive time points and then dividing by the total
number of state transitions excluding self-recurrences. Various definitions exist for transition
matrices (e.g., whether to use the number of occurrences or the probability, whether to
calculate the overall probability of 1 or the probability from a certain "from" state, and whether
to allow self-recurrence to the same label). Here we employed a transition probability with all
transitions except self-recurrences set to 1, to focus on the switching of a certain electric field
pattern, i.e., the ease or difficulty of switching in the neural network. Readers may refer to the
supplementary materials for results when other transition matrix definitions were applied.

2-1-4. Statistical analysis

In Study 1, we conducted an exploratory analysis of differences in EEG transition dynamics between younger and older adults. To explore the different characteristic transitions between older and younger groups, we calculated the effect size of the d family on the difference in transition probabilities for each transition in the two age groups (standardized mean difference obtained by dividing the difference in mean transition probability by the standard deviation of the two groups pooled; Hedge's g), as described by Zanesco et al. (2020). For differences in transition probabilities between age groups, we treated effect sizes greater than or equal to the required effect size determined by power analysis as "meaningful differences" (Zanesco et al., 2020). We conducted power analysis using G*Power 3.1.9.7 to evaluate the sensitivity in the difference between the two age groups. Power analysis revealed that an effect size $\gtrsim 0.44$ could be detected with an alpha error probability of 0.05, a power (1-β) of 0.8, and sample sizes of 60 and 130 for the older and younger age groups, respectively.

In addition to examining age differences in the transition probability of each transition pair, we conducted a principal component analysis (PCA) on the number of transitions for all 100 transitions for all participants to characterize the microstate transitions. Applying scaling and centering to the number of counted transitions and then PCA, the inter-participant correlation matrix for the number of transitions for all 100 transition pairs was transformed into an uncorrelated composite variable. We then applied Varimax rotation after PCA to examine the dimensional structure along the original data structure and improve the data's interpretability. PCA was performed in RStudio version 2021.09.0 and R version 4.3.1 (R Core Team, 2023) using the R function "*prcomp*." Subsequently, the relationship between the age groups and the components of transitions was examined in both directions using logistic regression and multivariate t-tests (Hotelling's T^2 test), utilizing the R functions "*glm*" and "*HotellingsT2Test.*" We used the R function "*effectsize*" to calculate the Hedge's g for post hoc Welch's t-test. We applied Holm's method to adjust the significance level in multiple comparisons. Adj.p in the results section represents the adjusted p-value, obtained by dividing the conventional significance level of 5% by the number of comparisons for convenience.

2-2. Results

2-2-1. EEG microstate templates

After modified k-means clustering, five maps were extracted from all participants' eye-closed data, in line with the approach used by Zanesco et al. (2020). These five maps explained 78.21% of the GEV. This value was comparable to those observed in other studies: a previous review showed that microstate studies employing four cluster maps explained approximately 65–84% of the GEV (Michel & Koenig, 2018). We labeled them as microstates A, B, C, D, and E by careful visual inspection based on the labels unified in Tarailis et al. (2024) (Figure 1a). The spatial correlations between our templates and those of a previous study (Asai et al., 2022), which employed the four template maps A, B, C, and D, were sufficiently high (for microstates A–D, rs > .88; Figure 1b). Additionally, our microstate E had the highest correlation coefficient with microstate C among the four maps used by Asai et al. (2022) (r =.73), consistent with the findings of previous studies that microstates C and E had not previously been distinguished (e.g., Tarailis et al., 2021).

Next, to perform template-matching considering the topographical polarity of the maps comprising the EEG time series data, after identifying the k (k = 5) dimensional space, we decided to consider the positive and negative directions of each dimensional axis (i.e.,

topographical polarity). Microstates obtained by modified *k*-means clustering can be treated
as basis vectors of a subspace of the EEG channel space, i.e., all topographical states on that
basis vector show the same electric field pattern (Mishra et al., 2020). We tried to extend this
by treating the EEG microstate basis vector as an "oriented" vector that considers orientation.
A polarity-reversed map was created and added for each map obtained by the modified *k*-
means algorithm. Thus, ten maps were created that were used as microstate templates for
polarity-considering matching in this study (Figure 1c).
Furthermore, the positional relationship of each template map was identified based on
the distance between maps. Specifically, the positional relationship between maps was
determined by compressing the distances defined by the spatial correlation coefficients
between topographies (Figure 1d; i.e., dissimilarity matrix between topographies) in three
dimensions using the classical multidimensional scaling (MDS) method (Asai et al., 2023;
Koenig et al., 2024). We confirmed that when the topographical polarity was considered, the
EEG topographies containing EEG microstate templates, which were centroids of states in
specific categories, were arranged to cover the surface of the sphere (Figures 2a and 2b). The
relative positions of the 10 EEG microstate templates were revealed (Figure 2c).
404
2-2-2. Replication of previous findings when using the topographical polarity-ignored
microstate template maps
First, as a confirmation, we checked whether we reproduced the transition features of
the older and younger age groups shown in Zanesco et al. (2020) and many other previous
microstate studies, with polarity ignored in our analysis. Previous studies have demonstrated
that transitions to microstates C, D, and E were less common, and transitions related to
microstates A and B were more common in older than in younger adults (Jabès et al., 2021;
Tomescu et al., 2018; Zanesco et al., 2020). We performed a conventional microstate analysis
applying the five template maps (before adding inversion maps) and calculated the transition
probability matrices between the five category maps for the older and younger age groups.
The difference between the transition probability matrices for the age groups and their
standardized differences were then calculated. These transition probabilities were also
represented as directed graphs with each template map as a node and the frequency of
transitions between nodes or the magnitude of the difference between age groups as edges.
The five template maps explained an average of 69.78% (*SD* = 5.77) of the GEV of
each participant's EEG topographic time series. The total GEV could also be divided into
GEVs for each of the five categorical maps, with microstate A having a mean GEV of 11.37%
(*SD* = 4.08); B, 11.86% (*SD* = 4.28); C, 22.52% (*SD* = 10.32); D, 14.82% (*SD* = 6.19),; and E,
9.20% (*SD* = 4.44).
Figure 3 shows the matrix and directed graph of the transition probabilities of each age
group (Figures 3a and 3b), difference between each transition pair for both groups (older-
younger; Figure 3c), and standardized mean difference between age groups for each
transition pair (Figure 3d). In line with previous findings, we observed that transitions to
microstate C were less frequent in the older group than in the younger group. In particular, the
fewer transitions from microstates C to E, E to D, and D to C in the older group exceeded the
effect size detectable in Study 1 (|*d*| = 0.51-0.64).
In addition, transitions related to microstates A and B were conversely more common
in the older group than in the younger group. In particular, higher transition probabilities were
observed from microstates A to D, D to B, B to A, E to A, and B to E in the older group. These
exceeded the effect sizes detectable in Study 1 (|*d*|s = 0.44-0.87).

Interestingly, the directed graphs visualizing the transition matrices also revealed the
relative positional relationships among the template maps (Figure 3; see Figure 1d). As
depicted in Figure 3, based on the dissimilarities among the five template maps, the
topography of the 32-electrode space was compressed, and the five topographies were
embeddable in 2D. The relative position of the five template maps was the furthest distance
between microstates A and B, followed by microstates E and D. The axes connecting
microstates A and B, as well as E and D, were arranged in a cross shape, with distances A-E
and B-E, as well as distances A-D and B-D, nearly equal. On the other hand, when comparing
distances E-C and C-D, E-C was slightly further apart than C-D. Furthermore, microstate C
was located at the intersection of the two axes.

<u>2-2-3. EEG microstate transitions by considering the topographical polarity</u>
Next, we performed an extended microstate analysis, which incorporated template-
matching while accounting for topographical polarity. We could obtain ten polarity-considered
microstate templates by adding the polarity-reversed topographical maps to the clustering
maps (Figure 1c). This allowed us to subdivide transitions into several sub-transitions. For
example, the transition from A to B could be subdivided into four transitions: from A+ to B+,
from A+ to B-, from A- to B+, and from A- to B-. The ten templates were applied to the data,
as in section 2-2-2. This allowed us to obtain results on the transition probability matrices and
directed graphs among the ten templates for each age group and the differences between the
two groups.
First, the positional relationships among the ten templates were clarified in 3D state
space through classical MDS based on spatial correlations among template maps (Asai et al.,
2023; Koenig et al., 2024). The positions of five template maps of respective positive or
negative polarity were consistent with the results of the five templates without polarity (in
section 2-2-2; see Figure 3). Additionally, the templates with reversed polarity (e.g., A+ and
A-) were located opposite each other because the dissimilarity value was 2. Ten states were
placed on the 3-D compressed abstract space, as shown in Figure 4, and their position was
determined (see also Figure 4 and Figure S5 for the animation image).
Template matching using a total of 10 maps on average explained 69.78% (SD = 5.77)
of the GEV of the EEG topographic time series for each participant. The GEV of each
microstate label was as follows: microstate A+, 5.86% (SD = 2.09); B+, 6.15% (SD = 2.29);
C+, 11.60% (SD = 5.48); D+, 7.71% (SD = 3.38); E+, 4.74% (SD = 2.34); A-, 5.51% (SD =
2.01); B-, 5.70% (SD = 2.02); C-,10.92% (SD = 4.89); D-, 7.11% (SD = 2.86); and E-, 4.46%
(SD = 2.13).
Figure 4 shows the matrix and directed graph of the averaged transition probabilities
of the older and younger groups (Figures 4a and 4b), subtraction results between age groups
(older-younger; Figure 4c), and standardized mean difference between age groups for each
transition pair (Figure 4d). The results suggested that considering topographical polarity during
the template-matching process extended the previous findings. When considering the
topographical polarity, it was observed that not all of the sub-transitions occurred equally, but
there was a bias in the transition probabilities that occurred. For example, transitions from/to
C were restricted within the same polarity. Transitions between topographical polarities
basically rarely occurred (see the upper right and lower left segments of the transition
probability matrices in Figures 4a and 4b). However, some specific transitions (i.e., between
A and B, as well as between D and E) were limited to transitions between polarities. For
example, transitions from A to B were limited to those from A+ to B- (averaging 3.6% in the
younger group and 3.7% in the older group) or from A- to B+ (averaging 3.6% in the younger

group and 3.6% in the older group), while transitions from A+ to B+ (averaging 0.0% in the
younger group and 0.1% in the older group) or A- to B- (averaging 0.0% in the younger group
and 0.1% in the older group) were rarely observed.

Regarding the differences between older and younger adults, it was reproduced that
transitions between microstates C, D, and E were less frequent and that transitions associated
with microstates A and B were more common in the older group. Such differences were
restricted to topographical polarity: for transitions involving microstates C, D, and E, within-
polarity transitions (C-D and C-E) and between-polarity transitions (D-E) were observed less
frequently in older adults (with effect sizes above detectable thresholds, transition of
microstates D+ to C+: $|d|$ = 0.45; C+ to E+: $|d|$ = 0.63; E+ to D-: $|d|$ = 0.61; D- to C-: $|d|$ = 0.56;
C- to E-: $|d|$ = 0.65; E- to D+: $|d|$ = 0.56). Plotting these on the neural manifold suggested a
circle-shaped decreasing transition route connecting D-C-E sequentially between polarities
(Figures 4c and 4d). The C, D, and E-related transitions other than the above, such as
between-polarity C-E and C-D transitions or within-polarity D-E transitions, were not
significantly reduced among older participants.

Conversely, transitions involving microstates A and B were notably more frequent
within the same polarity, primarily characterized by increased transition from A to D (positive:
$|d|$ = 0.93; negative: $|d|$ = 0.80), D to B (positive: $|d|$ = 0.72; negative: $|d|$ = 0.67), B to E
(positive: $|d|$ = 0.44; negative: $|d|$ = 0.45), and E to A (within positive polarity: $|d|$ = 0.58; within
negative polarity: $|d|$ = 0.53) in older participants (Figures 4c and 4d). Transitions from B+ to
A- and B- to A+ were also more common among older participants ($|d|$s = 0.55 and 0.58,
respectively).

Furthermore, a characteristic feature of the transitions in older participants was the
increased occurrence of transitions that were rare. Specifically, within-polarity transitions
between A and B ($|d|$s = 1.16 to 1.29), transition from E- to D- ($|d|$ = 0.65), transition from D-
to A+ ($|d|$ = 0.62), and transitions between opposite same-label states (between A±: $|d|$s =
0.88-0.93; between B±: $|d|$s = 0.84-0.91; from E+ to E-: $|d|$ = 0.46), were more common in
older than in younger adults.

The number of nodes in the direction between polarities was lower for the 10 templates
created in the data-driven manner than in the other axes. Therefore, to ensure accuracy, we
further verified the transition matrices using 14 templates, incorporating artificial midpoints
between A+ and B+ (designated as Ab), A- and B+ (designated as aB), D+ and E- (designated
as De), and D- and E+ (designated as dE). This adjustment was made to ensure that the
distances between the transition nodes on the sphere were approximately equal (cf., Figure
2c). As a result, the transition trends observed in the 10 templates were robustly reproduced
(Figure 5).

To clarify the effect of considering topographical polarity on age group differences, we
also compared the transition probabilities for each within- and between-polarity transition from
one state to another. We simplified the options of "to" states into two and recalculated the
transition probabilities (Figure 6): within- or between-polarity transitions. For within-polarity
transitions, we found a significant T^2 effect (T^2 = 42.26, df = 10, p < .001). Post-hoc analysis
revealed that the older group was more likely to transition from microstate A± to other states
of the same polarity (A+: t(116.93) = 4.86, p < .001, adj.p < .001, g = 0.75; A-: t(128.32) = 3.72,
p < .001, adj.p = .002, g = 0.55) while less likely to within-polarity transition from microstate
C± (C+: t(108.36) = -4.29, p < .001, adj.p < .001, g = 0.68; C-: t(114.24) = -5.04, p < .001, adj.p
< .001, g = 0.79). For inter-polar transitions, we found a significant T^2 effect (T^2 = 23.11, df =
10, p = .01). Post-hoc analysis revealed that the older group was more likely to between-

530 polarity transition from B± (i.e., mostly from B± to A∓; B+: $t(95.22) = 3.63$, $p < .001$, adj.$p = .005$,
531 $g = 0.61$; B-: $t(95.40) = 3.59$, $p < .001$, adj.$p = .005$, $g = 0.61$) and less likely than the younger
532 group to make an inter-polar transition from E (i.e., mostly from E± to D∓; E+: $t(164.47) = -$
533 2.94, $p = .004$, adj.$p = .03$, $g = 0.40$; E-: $t(159.07) = -2.62$, $p = .01$, adj.$p = .07$, $g = 0.36$).
534
535    <u>2-2-4. Transition components based on inter-participant correlation of transition</u>
536 <u>probabilities</u>
537    We performed PCA using the inter-participant correlation matrix for the counts of each
538 transition pair (Figure 7). Based on parallel analysis, eight components were employed (Figure
539 8a); these eight PCs explained 87.65% of the variance in the data (Figure 8b). After PCA,
540 Varimax rotation was applied to the PCA results to interpret each PC. Each transition pair was
541 grouped as belonging to the component with the highest absolute value of rotated component
542 loadings (see Table S1). The transition pairs contributing to each rotated component after
543 Varimax rotation are shown in Figure 8c. From the list of transition pairs contributing to each
544 rotated component, each component was interpreted and named as follows. Rotated PC1 was
545 named "Hub C" because it was a set of transitions between C (C+/C-) and the opposite ABDE
546 and the self-recurrence of C. Rotated PC2 was named "Hub E" because most of the
547 contributing transition pairs were a set of transitions from/to E (E+/E-). Rotated PC3 was
548 named "E-C-D rotation" because most of the contributing transition pairs were a set of
549 transitions belonging to the one-directional transition routes E+, C+, D+, E-, C-, and D-.
550 Rotated PC4 was named the "A-D plane" because it was a set of transitions between A (A+/A-)
551 and D (D+/D-). Rotated PC5 was named the "B-D plane" because it was a set of transitions
552 between B (B+/B-) and D (D+/D-). Rotated PC6 was named "D-C-E rotation" because it
553 contained a transition route in the opposite direction of rotated PC3. Rotated PC7 was named
554 "A-C-B rotation" because it was a set of transitions belonging to one-directional transition
555 routes A+, C+, B+, A-, C-, and B-. Finally, rotated PC8 was named "B-C-A rotation" because
556 it was a set of transition routes in the opposite direction of rotated PC7.
557    Further, we conducted a multivariable logistic regression analysis to examine whether
558 these eight transition component scores predicted binomial age group (0 = younger, 1 = older).
559 For transition components where most transition pairs had negative loading values, the rotated
560 component scores were reversed (hub E, B-D plane, A-C-B rotation, and B-C-A rotation) to
561 align the relationship between age group transition components. The eight transition
562 component scores for the explanatory variables were composite scores based on Varimax
563 rotated PCA, so multicollinearity did not occur (VIFs were 1.02 to 1.23). The overall model
564 demonstrated good fitness and appropriate explanatory variables were included, as evidenced
565 by a non-significant Hosmer-Lemeshow chi-squared goodness-of-fit (GOF) test ($X^2(8) = 11.52$,
566 $p = .17$). The Nagelkerke pseudo-R-squared measure showed that all of the predictors
567 together explained 48% of the variance.
568    The results of the logistic regression analysis are shown in Table 1. All p values on
569 logistic analysis were determined using Wald's test. The model fit results revealed that "hub
570 E" (odds ratio (OR) = 2.98, $p < .001$, 95% CI = [1.88 4.73]), "A-D plane" (OR = 3.01, $p < .001$,
571 95% CI = [1.87 4.84]), "B-D plane" (OR = 2.29, $p < .001$, 95% CI = [1.44 3.64]), "D-C-E rotation"
572 (OR = 0.45, $p = .002$, 95% CI = [0.27 0.73]), and "A-C-B rotation" (OR = 2.01, $p = .002$, 95%
573 CI = [1.30 3.11]) were significant predictors of age groups. On the other hand, "hub C," "E-C-
574 D rotation," and "B-C-A rotation" components were not significant predictors.
575    This relationship between transition components and age groups was also confirmed
576 by a multivariate t-test (Hotelling's T^2 test) that examined whether there were differences in

each transition component score by age group (Figure 9). We found a significant T^2 effect (T^2
= 102.12, *df* = 8, *p* < .001). Post-hoc analysis revealed that the older group showed the larger
transition component score of "B-D plane" (*t*(107.11) = 3.57, *p* < .001, adj.*p* = .003, *g* = 0.57),
"hub E" (*t*(88.95) = 4.19, *p* < .001, adj.*p* < .001, *g* = 0.73), "A-D plane" (*t*(88.54) = 4.13, *p* < .001,
adj.*p* < .001, *g* = 0.72). Also, larger "A-C-B rotation" (*t*(90.96) = 2.38, *p* = .02, adj.*p* = .08, *g* =
0.41) in the older group was marginally significant. On the other hand, less "D-C-E rotation" in
older group was marginally significant (*t*(116.31) = -2.59, *p* = .01, adj.*p* = .055, *g* = 0.40).
584

2-3. Discussion
Study 1 updated the EEG microstate analysis by considering topographical polarity.
We investigated whether this approach is practical when comparing differences in EEG
spatiotemporal transition dynamics between older and younger adults. First, the decreased
transitions to C and the increase in A- and B-related transitions in older people shown in
previous studies (e.g., Zanesco et al., 2020) were replicated and extended in the present study.
Interestingly, these age-related transitions were limited to certain sub-transitions when
topographical polarity was considered. Specifically, for the transitions related to microstates
C, D, and E, which were less frequent in the older group, a decrease in transitions in the older
group mainly occurred between microstates C and D/E of the same topographical polarity as
C (especially D± to C± and C± to E±) and between microstates D and E of opposite polarity
(especially E± to D∓). Conversely, for transitions related to microstates A and B, which were
dominant in the older group, the increase in transitions mainly occurred within the same
topographical polarity and some between polarities. These results suggest that microstate
discrete transitions have specific fixed routes and that the frequency of passing among these
routes changes with aging.
These transitions within and between polarities depended on the placement of the EEG
topography on the neural manifold. If we reformulate the description of EEG dynamics using
EEG microstates as a problem of segmentation of the spherical surface and the transition
between the segmented areas (Asai et al., 2023), we showed that ten microstates can be
placed in a fixed relative position. This finding is not limited to the case of ten microstate maps
but can be extended to any number of microstates if the topographical polarity is considered
(i.e., the question of how many divisions of the sphere to make). As a result, the distribution
of areas corresponding to microstate C was such that other states of the same polarity
surrounded them. Such an arrangement limited the transitions involving C in successive two-
state transitions to transitions within the same polarity. Also, areas corresponding to A+ and
B-, A- and B+, D+ and E-, and D- and E+, where relatively frequent transitions between
polarities were observed, were adjacent on the neural manifold space.
The perspective of transitions within and between the topographical polarity,
developed by polarity-sensitive fitting, may help describe differences between older and
younger groups. The results of this study suggested that between-polarity transitions can
occur in only a very limited pattern, although statistical significance could not be determined
due to the exploratory nature of the analysis. These limited between-polarity transitions,
especially E± to D∓, were less common in the older group than in the younger group. Also,
reduced transitions to C have been treated as a characteristic of microstates in older adults,
but C-related transitions were limited to within the same polarity. These results suggested that
the transition decrease on the axis connecting microstates D-C-E, especially the reduced
within polarity D-C and C-E transitions and between-polarity E-D transitions, were
characteristic of older people. Furthermore, for A and B-related transitions, the difference

between younger and older was in the many transitions among the older between microstates
A-D-B-E within the same topographical polarity and between-polarity transition from B to A.
Rare transitions were also greater in older adults. Therefore, fewer transitions circling the D-
C-E axis, more A-D-B-E within-polarity transitions and B-A between-polarity transitions, and
more rare transitions may be biomarkers of aging.
The advantage of considering topographical polarity became more obvious when we
took a macroscopic view of transitions from one state to another within or between polarity
states. The results of Study 1 indicated differences by age group in the within-polarity
transitions from microstates A and C and the between-polarity transitions from microstates B
and E. Although our definition of topographical polarity is arbitrary, it appears that both "which
country is it currently in (i.e., state)" and "which direction is being travelled (i.e., within and
between the polarity)" affect the EEG dynamics with age.
These aging features of microstate transitions were also expressed consistently in the
rotated components, separated by transitional features. In this study, discrete transitions were
divided into eight components that followed the trajectories on the neural manifold, drawn on
the assumption of continuous neural dynamics. These were divided into transitions originating
from/to C; transitions originating from/to E; transitions such as moving on a plane containing
A and D, as well as B and D; and rotational transitions with a specific direction. Interestingly,
among these components, fewer transitions originating from E, fewer transitions between B
and D, fewer rotational transitions in the D-C-E and A-C-B directions, and more transitions
between A and D were significant predictors of aging.
Among the significant predictors, the component of E-related transitions had the
largest explained variance, indicating that transitions connecting to other states with E as a
hub are less common in the older group, alongside transitions to C. Microstate E, the fifth state
after the four canonical states, may be essential for explaining differences in aging. Although
the hub C component did not significantly predict aging, our hub C includes self-recurrences
of C and C-related between-polarities transitions, which rarely occur. The fewer transitions to
C in the older group are likely reflected in two rotational components, D-C-E and A-C-B rotation.
Our findings suggest that the transitions that change with aging are directional. Furthermore,
the components capturing transitions between microstate D and passive microstates (i.e., A
and B), which are said to be associated with sensory processing (Britz et al., 2010), also
changed with aging. These may also reflect a limited hub function of D that was previously
unknown. However, these findings are exploratory and need to be validated on another
dataset to assess the robustness of these aging features.
658
659   **3.** **Study 2: Confirmatory analysis of age-related transition differences**
660
Study 2 examined whether the age-related differences in resting EEG state transition
dynamics observed in Study 1 represent stable and robust features. To achieve this goal, we
examined the reproducibility of the results of Study 1 using independent data.
We applied the updated microstate analysis using our younger-older resting-state
spontaneous EEG dataset. Based on the transitions that showed meaningful effect sizes
(Hedge's g) in Study 1, we tested the following hypotheses regarding EEG state transitions in
the older group: (a) fewer transitions on the D-C-E axis across polarity, especially fewer within-
polarity transitions from D to C and C to E, and between-polarity transitions from E to D; (b)
more within-polarity transitions among A, D, B, and E, especially from A to D, D to B, B to A,
and between-polarity transitions from B to A; and (c) more rare transitions, especially from E-
to D-, D- to A+, E+ to E-, between A±, between B±, and between A-B. When those transitions

were crudely categorized into within- and between-polarity transitions, we examined whether
they could also be replicated that the older group had more transitions from A± and fewer
transitions from C± to within-polarity states than the younger group, as well as more from B±
and fewer from E± to between-polarity transitions. We also verified whether the co-occurrence
structure of transitions found in Study 1, referred to as transition components, could be
confirmed in another dataset. We then confirmed whether those transition components could
distinguish age groups, i.e., transitions with E as a hub, transitions connecting passive
microstates and D, and unidirectional D-C-E and A-C-B rotation components.
680
3-1. Methods
3-1-1. Participants
Thirty-five healthy adults participated in the experiment. Participants were categorized
into two age groups: sixteen younger participants aged 20–40 years comprised the younger
group (7 females, 9 males, mean age = 26.0 years, SD = 6.0), and 19 older participants aged
61–80 years comprised the older group (9 females, 10 males, mean age = 70.5 years, SD =
5.3). All participants gave informed consent before the experiment and provided written
consent to participate and share data. This study was approved by the local ethics committee
(reference number 19-144 for the Ethics Committee of ATR).
Of the 35 participants, 3 older participants who could not complete all tasks correctly
(due to interruption, remeasurement, or repetition of some of the experimental tasks) were
excluded from the analysis. Therefore, 32 participants were included in the analysis. The
younger group comprised 16 participants (7 females; 9 males; mean age = 26.0 years, SD =
6.0; age range, 20–40 years). The older group also comprised 16 participants (6 females; 10
males; mean age = 70.4 years, SD = 5.0; age range, 61-79 years).
696
3-1-2. Experimental settings and procedures
The data were collected as part of another research project on brain function in older
individuals, conducted between November 2018 and July 2019. EEG and fMRI data were
recorded while participants performed several cognitive tasks on different occasions. During
the EEG recording session, participants were asked to perform six different tasks for six
minutes per task. The six tasks included four eye-closed tasks (rest, meditation, heartbeat
counting, and breath counting) and two eye-open tasks (rest and meditation). The order of the
tasks was fixed among the participants. We utilized the eye-closed resting-EEG data in this
study.
During the eye-closed resting EEG measurement, participants were instructed to sit in
a comfortable chair and remain at rest with their eyes closed, minimizing active thought as
much as possible.
709
3-1-3. EEG data collection, preprocessing, and EEG microstate analysis
EEG signals were recorded using 32 silver-silver chloride electrodes on saltwater
sponge-based electrode caps (R-net 32ch, Brain Products GmbH, Gilching, Germany). The
32 electrodes were placed at Fp1, Fp2, Fz, F3, F4, F7, F8, F9, F10, FC1, FC2, FC5, FC6, Cz,
C3, C4, T7, T8, CP1, CP2, CP5, CP6, Pz, P3, P4, P7, P8, P9, P10, Oz, O1, and O2, according
to the international 10-10 systems. Reference and ground electrodes were placed at FCz and
Fpz, respectively. Impedance was kept below 50 kΩ. EEG signals were amplified with an
online bandpass of 0.016-250 Hz and digitized using BrainAmp (Brain Products GmbH,
Gilching, Germany) at a sampling rate of 500 Hz.

The EEG data underwent the same preprocessing and microstate analysis as those in
Study 1. Other than the difference in the data used, no modifications were made to the analysis
parameters. However, to avoid the influence of microstate template differences between
studies, which is one of the reasons for unstable EEG microstate analysis results (Koenig et
al., 2024; Tarailis et al., 2024), we used the same EEG microstate templates in Study 2 created
from the LEMON dataset in Study 1. Specifically, we first reduced the template data to 28
electrodes, which were shared electrodes between Studies 1 (61 channels) and 2 (32
channels). The position of each electrode was commonized based on MNI coordinates.
Subsequently, the F9, F10, P9, and P10 electrodes, absent in the LEMON data but included
in our data, were interpolated using the EEGLAB function "*pop_interp*." Following this, the
EEG microstate templates adjusted for our R-net data were acquired.
730
3-1-4. Statistical analysis
In Study 2, we confirmed the results obtained in Study 1. The methods for calculating
transition probabilities and standardized mean differences were the same as in Study 1. We
conducted a multivariate Hotelling's T^2 test, which tests the difference between two
multivariate groups with a chi-square approximation based on each of the following three
hypotheses found in Study 1: (a) in older groups, fewer transitions on the D-C-E axis including
between-polarity transitions are observed, especially, from D± to C±, C± to E±, and E± to D∓;
(b) greater transitions between A-D-B-E (eight within-polarity transitions from A± to D±, D± to
B±, B± to E±, E± to A±, and between-polarity transition from B± to A∓); (c) fewer rare transitions
from E- to D-, D- to A+, E+ to E-, between A+ and A-, B+ and B-, and A± and B±. Statistical
analysis was conducted using RStudio version 2021.09.0 and R version 4.3.1 (R Core Team,
2023). The R functions "*HotellingsT2Test*" and "*effectsize*" were utilized for the multivariate *t*-
tests and post hoc Welch's *t*-test. We applied Holm's method to adjust the significance level
in multiple comparisons. Adj.*p* in the results section represents the adjusted *p*-value, obtained
by dividing the conventional significance level of 5% by the number of comparisons for
convenience.
To further investigate the robustness of the co-occurrence transition structure found in
Study 1, the eigenvectors and the rotation matrix obtained in Study 1 were applied to the data
in Study 2. Then, as in Study 1, we reorganized the rotated components based on the
maximum loadings of each transition pair. Logistic regression analysis elucidating the age
groups and Hotelling's T^2 test were also conducted using the rotated components obtained in
Study 2.
753
3-2. Results
3-2-1. EEG microstate fittings and transitions by considering the topographical polarity
We performed an extended microstate analysis by matching the EEG microstate
templates created in Study 1 to the data in Study 2. The results showed that the template
maps from Study 1 explained an average of 68.51% (*SD* = 6.29) of the GEV of each
participant's EEG topography time series in Study 2: each microstate label explained 7.42%
(*SD* = 2.52) for microstate A+, 5.77% (*SD* = 2.21) for B+, 10.67% (*SD* = 4.98) for C+, 7.54%
(*SD* = 4.73) for D+, 3.78% (*SD* = 1.67) for E+, 7.02% (*SD* = 2.37) for A-, 5.56 % (*SD* = 2.06)
for B-, or C-, 6.89% (*SD* = 4.07) for D-, and 3.64% (*SD* = 1.51) for E-.
We calculated the transition probabilities between ten states and the differences
between each age group. Figure 10 presents the matrices and directed graphs of transition
probabilities by older and younger age groups (Figures 10a and 10b), the subtraction results

between age groups for each transition pair (older-younger; Figure 10c), and the standardized
mean differences between age groups for each transition pair (Figure 10d; also see
supplementary Figures S14–16 for additional results using alternative transition matrix
definitions).
First, we examined whether there was more than one mean difference between the
age groups concerning transitions on the D-C-E axis, for which we found promising differences
in Study 1. The results showed a significant T^2 effect (T^2 = 16.20, degree of freedom (df) = 6,
p = .01). Post-hoc analysis revealed that some transition probabilities were significantly lower
in the older group: the transitions from C+ to E+ (t(27.01) = -3.02, p = .005, adj.p = .03, g =
1.04) and C- to E- (t(24.97) = -2.95, p = .007, adj.p = .03, g = 1.02).
Second, regarding the hypothesis about transitions among A-D-B-E, we found a
significant T^2 effect (T^2 = 52.67, df = 10, p < .001). Specifically, transition probabilities were
more frequent in the older group for the transitions from A+ to D+ (t(29.77) = 4.99, p < .001,
adj.p < .001, g = 1.72); D+ to B+ (t(29.06) = 3.40, p = .002, adj.p = .01, g = 1.17); A- to D-
(t(28.46) = 5.09, p < .001, adj.p < .001, g = 1.75); and D- to B- (t(29.38) = 4.01, p < .001, adj.p
= .003, g = 1.38).
Finally, for the third hypothesis about rare transitions, we also found a significant T^2
effect (T^2 = 30.91, df = 11, p = .001). Post-hoc analysis revealed that the transition from A+ to
B+ (t(29.63) = 3.02, p = .005, adj.p = .06, g = 1.04) significantly increased in the older group.
In addition, we conducted an exploratory analysis to investigate transitions other than
the transition pairs that had promising differences in Study 1. Power analysis using G*Power
3.1.9.7 revealed that an effect size > 1.02 could be detected with an alpha error probability of
0.05, a power of 0.8, and a sample size of 16 participants per group. From Figure 10d, in
addition to the hypotheses, several of the transitions from/to C± within and between polarities
were less common in the older group: C+ to B+, C+ to B-, C+ to E-, C- to B+, and C- to C+
($|d|$s = 1.04 to 1.82). Also, concerning the hypothesis about the transitions on the A-D-B-E
axis, the transition from D- to A- was more frequent in the older group ($|d|$ = 1.04).
In the age-group comparison of the transition probabilities from one state to each of
the within- and between-polarity states (Figure 11), based on the results of Study 1, we
investigated whether age differences were observed in (d) within-polarity transitions from A±,
(e) within-polarity transitions from C±, (f) between-polarity transitions from B±, and (g)
between-polarity transitions from E±, using Welch's t-test. For (d), a marginally significant
higher within-polarity transition from A+ was observed in the older group (t(29.80) = 1.70, p
= .099, g = .59), and no significant difference was found from A- (t(30.00) = 1.12, p = .27, g
= .39). For (e), within-polarity transitions from C± were significantly lower for older adults (C+:
t(28.70) = -3.70, p < .001, g = 1.27; C-: t(27.16) = -3.32, p = . 003, g = 1.15). On the other
hand, for (f) and (g), no significant differences were observed between age groups (B+:
t(28.35) = -1.11, p = .28, g = .38; B-: t(27.71) = -0.71, p = .49, g = .24; E+: t(29.66) = -0.84, p
= .41, g = .29; E-: t(30.00) = -0.76, p = .46, g = 0.26).
805
3-2-2. PCA based on the data structure observed in Study 1 and logistic regression
analysis for age differences
In Study 2, with 100 transitions, we aimed to assess the contribution of each transition
pair to each component in the PC state space identified in Study 1. To achieve this, we first
calculated component scores using the eigenvectors obtained in Study 1. Assuming the same
eight-dimensional structure as in Study 1, the eight PCs could explain 78.29% of the entire
Study 2 data. Subsequently, the rotated component loadings and scores were calculated using
the rotation matrix from the Varimax rotation of the eight-dimensional PC space in Study 1

(Table 2). Each transition pair was considered to contribute to the rotated component with the
largest absolute loading values. Figure 12 shows the transition components in Study 2 using
the weight matrix defined in Study 1. Based on the group of transition pairs contributing to
each of the eight rotational components, the eight components were almost congruent with
"hub C," "E-C-D rotation," "B-D plane," "hub E," "D-C-E rotation," "A-D plane," "A-C-B rotation,"
and "B-C-A rotation" in Study 1.

Furthermore, multivariate logistic regression analysis predicting age groups (0 = young,
1 = old) from the eight transition component scores showed a non-significant Hosmer-
Lemeshow chi-square GOF test result ($X^2(8) = 8.60$, $p = .38$) for the overall model. This
indicates a good fit of the model and the inclusion of appropriate explanatory variables.
Nagelkerke pseudo-R-square measures showed that all predictors together explained 73% of
the variance. Multicollinearity did not occur because VIF ranged under 10 (1.34–8.74). The
logistic regression analysis revealed that "A-D plane" was a significant predictor of age groups
(OR = 16.21, $p = .04$, 95% CI = [1.15 228.75]).

The relationship between transition components and age groups was confirmed by
Welch's t-test for each of the five transition component scores, the differences of which were
found in Study 1 (Figure 13). The results showed a significant age-group difference in "A-D
plane" scores, which was higher in the older group ($t(27.99) = 2.69$, $p = .01$, $g = .93$). The "D-
C-E rotation" score was marginally significant, lower in the older group than in the younger
group ($t(29.99) = -1.96$, $p = .06$, $g = .67$). On the other hand, no significant differences were
found for "Hub E" ($t(27.93) = 0.75$, $p = .46$, $g = .26$), "B-D plane" ($t(29.40) = 0.79$, $p = .43$, g
= .27), and "A-C-B rotation" ($t(29.35) = -1.21$, $p = .24$, $g = .42$). We further examined age group
differences for the three non-hypothetical components. We found a significant T^2 effect (T^2 =
10.23, $df = 3$, $p = .02$). Post-hoc tests revealed that the "Hub C" score was lower in the older
group ($t(29.98) = -2.75$, $p = .01$, adj.$p = .03$, $g = .95$). "E-C-D rotation" ($t(25.29) = -0.64$, $p = .53$,
adj.$p = .53$, $g = .22$) and "B-C-A rotation" ($t(24.43) = -2.04$, $p = .052$, adj.$p = .104$, $g = .70$) were
not significantly different.

3-3. Discussion

In Study 2, we attempted to confirm that the EEG microstate features suggested in
Study 1 are robust enough to be reproduced using an independent data set. As in Study 1,
we performed a polarity-sensitive EEG microstate analysis. We examined three hypotheses
on the difference of transition probabilities between age groups based on the results of Study
1: (a) transitions on the D-C-E axis across polarity are less common in the older age group,
(b) transitions between A-D-B-E within polarity are more common in the older age group, and
(c) rare transitions are more common in the older age group.

The first hypothesis regarding fewer transitions on the D-C-E axis in the older group
was partially supported. Based on the observations of Study 1, the transition groups, including
transitions from D± to C±, C± to E±, and E± to D∓ were less common in the older group than
in the younger group. In particular, within-polarity transitions from D to C and C to E were less
frequent in the older group than in the younger group. In contrast, between-polarity transitions
between E and D were not significant in Study 2. This suggests that the fixed routes that were
unlikely to transition with aging, especially within-polarity transitions between C and D/E at the
same polarity, are robust routes that show the effect of aging on transitions.

The second hypothesis regarding the A-D-B-E transition was also supported, as within-
polarity transitions from A to D and D to B were more frequent in the older group than in the
younger group. The transitions among A-D-B-E were mainly restricted to the polarity,

suggesting that the increase in A/B-related transitions found in previous studies may have occurred within this limited polarity. On the contrary, the third hypothesis was not supported, at least in Study 2, and no evidence was presented that the unnatural change in transitions (such as "jumping" between polarities when recorded at a sufficient sampling rate) reflects the effects of aging. The dataset for Study 2 was small but independent of that of Study 1. These results, observed in both Studies 1 and 2, indicated that fewer transitions along the D-C-E axis and more transitions among A-D-B-E within the same polarity are potential biomarkers of aging.

In addition, the results of Study 1 were partially replicated when focusing on transitions from one state to another within the same polarity and between polarities. In particular, the within-polarity transitions from A+ and C± are likely to be biomarkers of aging. On the other hand, no age-related differences were observed in Study 2 for between-polarity transitions from B and E. Despite the potential for undetected differences due to the low power of detection caused by the small sample size in Study 2, at least the within- and between-polarity transition routes from specific states were modulated by aging. Specifically, fewer transitions from A+ and more transitions from C± to within-polarity states are considered to be characteristic of EEG dynamics that change with age.

Furthermore, this study revealed that individual transitions can be grouped into similar transition units based on their co-occurrence relationships, named transition components. The transition components were a robust structure obtained independently of the dataset. They were divided into hubs at C and E, transition groups moving between A/B and D, and unidirectional rotational transition groups with directionality for the D-C-E and A-C-B axes. The cohesion of these transition components has the potential to capture the global EEG transition dynamics rather than problematizing individual transitions.

These transition components may be related to our cognitive functions, mental or physical states, and characteristics. In the present study, we attempted to explain age differences using eight transition component scores. Among the five significant predictors of age identified in Study 1 ("hub E," "A-D plane," "B-D plane," "D-C-E rotation," and "A-C-B rotation"), only "A-D plane" was significant across datasets. Nonetheless, considering that the number of events per variable generally needs to be greater than 10 (Peduzzi et al., 1996), the present dataset would have required a sample size of at least 10 for each of the eight variables or at least 80 samples. However, there were only 16 participants in each age group. The logistic regression results of Study 2 should be interpreted with caution. The comparison of mean transition component scores of each age group, which partially replicated Study 1, with "A-D plane" scores being higher and "D-C-E rotation" being lower in the older group, had very large standard errors overall, suggesting that there were issues in terms of statistical power. At this time, we reserve the conclusion that the transition components found in this study may reflect our psychological, bodily, or other aspects. This should be further investigated in future studies.

4. <u>General Discussion</u>

This study demonstrated that a state-of-the-art microstate analysis considering topographical polarity was appropriate for elucidating differences in EEG transition dynamics with aging. Using a careful two-step approach, we found that when topographical polarity and relative geography among microstates were considered, the older group showed fewer transitions on the D-C-E axis and more frequent transitions among A-D-B-E. Specifically, within-polarity transitions from a particular state were modulated. Moreover, our study

indicates that EEG microstate transitions can be decomposed into transition components
based on co-occurrence. Age-related changes in microstate transitions may increase or
decrease within a larger dynamic context, termed "topographical polarity" in this study. The
extended polarity-sensitive microstate analysis we proposed revealed the spatiotemporal
continuous transition dynamics, suggesting the significance of polarity-sensitive fitting in
microstate analysis.

The age-related differences in polarized microstate transitions in this study may reflect
age-related changes in brain structures and networks. Accumulated studies have shown that
aging is not only associated with cognitive abilities (e.g., Hedden & Gabrieli, 2004; Mather,
2010; Spreng & Turner, 2019; Tucker-Drob et al., 2019; Verhaeghen & Cerella, 2002) but also
with various changes in the brain (e.g., Aron et al., 2022; Cleeland et al., 2019; Li et al., 2001;
Oschwald et al., 2019; Samson & Barnes, 2013). For example, aging changes resting-state
functional connectivity (Ferreira & Busatto, 2013; Ferreira et al., 2016; Geerligs et al., 2015;
Sala-Llonch et al., 2015) and brain structure (Good et al., 2001; Lebel et al., 2010; Oschwald
et al., 2019; Resnick et al., 2003). Previous functional neuroimaging studies have proposed
age-related changes in gradient patterns, such as antero-posterior and supero-inferior
gradients (Boban et al., 2022). For instance, the posterior-anterior shift in aging is a well-
known phenomenon, characterized by reduced occipital activity and increased frontal activity
(Andrews-Hanna et al., 2007; Davis et al., 2008; McCarthy et al., 2014). This shift is said to
be characterized by functional compensation (Davis et al., 2008; Zhang et al., 2017).
Additionally, this shift has been observed in structural changes, such as alterations in white
matter (Head et al., 2004), and network dynamics (Andrews-Hanna et al., 2007; Zhang et al.,
2017). The age-related modulation of microstate transitions on the D-C-E or A-D-B-E axis
observed in this study is only a change in the electric field pattern in the topography of scalp
EEG. Therefore, it cannot be matched to brain regions observed in imaging studies. However,
the well-known structural and network constraints on the direction of information processing
in fMRI studies might be manifested as more or less transitions in the microstate transitions
on the D-C-E and A-D-B-E axes.

The transitions on the D-C-E axis, which were suggested to be modulated by aging in
this study, are state transitions along the midline of the scalp EEG. Studies of age-related EEG
changes have often reported findings of age-related attenuation of frontal midline theta activity.
Such changes in midline EEG oscillation may be related to aging (Tóth et al., 2014). Our
results extend these findings to suggest that EEG oscillation in the midline region may be
modulated not only in the time domain but also in the mass domain in relation to aging. Our
results pertain specifically to the pattern of supratentorial EEG. Examining the relationship with
the A-P gradient, as identified in brain imaging studies, would be valuable in future research.

Regarding electrophysiological neural aspects, researchers have primarily
concentrated on local changes in specific channels or frequency bands, as well as changes
in the time direction. For example, it is known that the alpha oscillation of resting EEG becomes
slow, and its power decrease with age (Babiloni et al., 2006; Chiang et al., 2011; Ishii et al.,
2017; Klimesch, 1999; Merkin et al., 2023; Scally et al., 2018; Tröndle et al., 2023). Additionally,
changes in EEG signal complexity have been observed with aging. Some studies have
reported increased complexity in older adults (Anokhin et al., 1996), while others have
reported reduced complexity (Lipsitz & Goldberger, 1992; Zappasodi et al., 2015). However,
the direction of change remains a topic for discussion due to the diversity of complexity indices
(Lau et al., 2022; Ma et al., 2021). Although our results represent only topographical transitions
recorded from supracranial EEG, polarity-sensitive microstate analysis allows us to represent
spatiotemporal continuous EEG transitions, which may reveal "easy/hard routes to transition"

constrained by brain structure and network proximity. Recent discussions in cognitive
neuroscience have shifted from the Sherringtonian approach, which elucidates the function of
individual brain regions and networks based on functional classification of neuronal
populations, to the Hopfieldian approach, which understands the neural basis of cognition from
the transition dynamics of masses encompassing local activities (Asai et al., 2022; Barack,
2021; Barack & Krakauer, 2021; Ebitz & Hayden, 2021). The polarized microstate approach
may be helpful in such a paradigm shift at the explanatory level.

Our results suggest that the polarity-neglected fitting traditionally employed in
microstate analysis may not be appropriate. Traditionally, two topographies of opposite
polarity have been considered due to the reversed activity of the same dipole and have been
neglected when considering the configuration of the electric field. Indeed, the results of this
study showed that the basic properties of the positive and negative polarity were very
symmetrical (e.g., the upper and lower triangular matrices of the transition matrix were
symmetrical). In this sense, our findings may support the validity of conventional microstate
analysis in terms of evaluating the average tendency of a particular electric field configuration
to emerge. However, in terms of discretized continuous transitions, this study suggests that
even the same D to E transition may have different frequencies of occurrence and even
meanings for the D+ to E+ and D+ to E- transitions. Therefore, our findings argued that the
two topographies of opposite polarity should be considered separately. At the very least,
polarity-sensitive microstate-fitting is helpful because it provides richer, more data-driven
information when we follow the neural dynamics, which are essentially continuous transitions.

The polarity of waveforms has originally been important in EEG research, including
event-related potential (ERP) studies. Although "polarity" in EEG microstate studies refers to
the positivity or negativity of the overall potential pattern at a given instant rather than the
polarity of a specific electrode waveform (referred to as "topographical polarity"), it has been
indirectly suggested for some time that polarity may have meaningful in microstate studies as
well. For example, Tamano et al. (2022) and Asai et al. (2022) suggested the oscillation of
EEG microstate dynamics and the existence of both topographical polarities. Moreover, our
observations, as well as those of many studies dealing with EEG topography during tasks not
restricted to microstates, indicate that EEG microstates during cognitive tasks seem to be
biased toward a particular pole, a pattern we call "negative." Further studies are needed to
examine whether each polarity state reflects something functional.

Another good point of the polarity-sensitive microstate fitting is that it allows us to
describe microstate dynamics as transitions on a closed loop system (i.e., sphere) in the space
of neural manifolds. Neural activity is essentially continuous, and the polarity-sensitive
microstate labeling is a good way to address such continuous dynamics as close to its essence
as possible, as a transition between divided domains on the surface of a sphere.

This study had several limitations that necessitate further investigation. First, defining
topographical polarity in this study posed a challenge. For convenience, the present study
referred to the positive microstates as patterns in which the frontal electrode group exhibited
positive and the occipital electrode group had negative potentials. Although this was an
arbitrary labeling, it is synonymous with calling bipolar global attractors that consequently
move between + and - based on the state distribution on the neural state space and transition
probability results. The present study suggests an increase in transitions limited within polarity
in older adults and limited transition routes across polarity. However, what function this
topographical polarity may have and what the transitions between + and − reflect remains
unclear. Further accumulation of findings on this point is awaited.

Second is the issue of the robustness of the transition components as reflecting
cognitive functions and mental states. In this study, we found eight transition components
based on the co-occurrence of 100 microstate transitions. However, it remains unclear how
stable these components are regardless of the technique and what the dynamics among
transition components are. In this study, the co-occurrence structure of transitions found in a
large public dataset acquired in Western countries is at least confirmed when the same
component axes were applied to a dataset acquired in Japan. However, it is uncertain whether
this structure will consistently emerge in Varimax rotated PCA. Further investigation is needed
to determine if these coherent units have any functional significance.

Previous studies on the functional roles of EEG microstates have primarily focused on
the functions associated with individual microstates. However, adopting the Hopfieldian
perspective, which attempts to explain cognition from the field dynamics, it may be worthwhile
to focus on the dynamics of transitions between states and even more abstract transition
components rather than the state of EEG microstates to explain cognition.

In summary, the present study revealed age-related differences in EEG transition
dynamics, using microstate analysis updated to account for topographical polarity. The
transition dynamics associated with aging were characterized by fewer transitions on the D-
C-E axis and more between-polarity transitions among A-D-B-E, as well as more transition
components associated with the A-D plane. The approach proposed in this study,
incorporating topographical polarity, may be useful for separating the conventionally
confounded easy and hard transitions and appropriately discretizing the spatiotemporally
continuous EEG dynamics.

5. <u>Reference</u>

Andrews-Hanna, J. R., Snyder, A. Z., Vincent, J. L., Lustig, C., Head, D., Raichle, M. E., & Buckner, R. L. (2007). Disruption of large-scale brain systems in advanced aging. *Neuron*, *56*(5), 924–935. https://doi.org/10.1016/j.neuron.2007.10.038

Anokhin, A. P., Birbaumer, N., Lutzenberger, W., Nikolaev, A., & Vogel, F. (1996). Age increases brain complexity. *Electroencephalography and Clinical Neurophysiology*, *99*(1), 63–68. https://doi.org/10.1016/0921-884x(96)95573-3

Antonova, E., Holding, M., Suen, H. C., Sumich, A., Maex, R., & Nehaniv, C. (2022). EEG microstates: Functional significance and short-term test-retest reliability. *NeuroImage: Reports*, *2*(2), 100089. https://doi.org/10.1016/j.ynirp.2022.100089

Aron, L., Zullo, J., & Yankner, B. A. (2022). The adaptive aging brain. *Current Opinion in Neurobiology*, *72*, 91–100. https://doi.org/10.1016/j.conb.2021.09.009

Artoni, F., Menicucci, D., Delorme, A., Makeig, S., & Micera, S. (2014). RELICA: A method for estimating the reliability of independent components. *NeuroImage*, *103*, 391–400. https://doi.org/10.1016/j.neuroimage.2014.09.010

Asai, T., Hamamoto, T., Kashihara, S., & Imamizu, H. (2022). Real-time detection and feedback of canonical electroencephalogram microstates: Validating a neurofeedback system as a function of delay. *Frontiers in Systems Neuroscience*, *16*, 786200. https://doi.org/10.3389/fnsys.2022.786200

Asai, T., Kashihara, S., Chiyohara, S., Hiromitsu, K., & Imamizu, H. (2023). Spatio-temporal "global" neurodynamics of the human brain in continuous and discrete picture: Simple statistics meet on-manifold microstates as multi-level cortical attractors. *bioRxiv*. https://doi.org/10.1101/2023.07.13.548951

Babayan, A., Erbey, M., Kumral, D., Reinelt, J. D., Reiter, A. M. F., Röbbig, J., Schaare, H. L., Uhlig, M., Anwander, A., Bazin, P.-L., Horstmann, A., Lampe, L., Nikulin, V. V., Okon-Singer, H., Preusser, S., Pampel, A., Rohr, C. S., Sacher, J., Thöne-Otto, A., … Villringer, A. (2019). A mind-brain-body dataset of MRI, EEG, cognition, emotion, and peripheral physiology in young and old adults. *Scientific Data*, *6*, 180308. https://doi.org/10.1038/sdata.2018.308

Babiloni, C., Binetti, G., Cassarino, A., Dal Forno, G., Del Percio, C., Ferreri, F., Ferri, R., Frisoni, G., Galderisi, S., Hirata, K., Lanuzza, B., Miniussi, C., Mucci, A., Nobili, F., Rodriguez, G., Luca Romani, G., & Rossini, P. M. (2006). Sources of cortical rhythms in adults during physiological aging: A multicentric EEG study. *Human Brain Mapping*, *27*(2), 162–172. https://doi.org/10.1002/hbm.20175

Barack, D. L. (2021). Mental kinematics: Dynamics and mechanics of neurocognitive systems. *Synthese*, *199*(1), 1091–1123. https://doi.org/10.1007/s11229-020-02766-1

Barack, D. L., & Krakauer, J. W. (2021). Two views on the cognitive brain. *Nature Reviews. Neuroscience*, *22*(6), 359–371. https://doi.org/10.1038/s41583-021-00448-6

Boban, J., Thurnher, M. M., Boban, N., Law, M., Jahanshad, N., Nir, T. M., Lendak, D. F., & Kozic, D. (2022). Gradient patterns of age-related diffusivity changes in cerebral white matter. *Frontiers in Neurology*, *13*, 870909. https://doi.org/10.3389/fneur.2022.870909

Britz, J., Van De Ville, D., & Michel, C. M. (2010). BOLD correlates of EEG topography reveal rapid resting-state network dynamics. *NeuroImage*, *52*(4), 1162–1170. https://doi.org/10.1016/j.neuroimage.2010.02.052

Chang, C. Y., Hsu, S. H., Pion-Tonachini, L., & Jung, T. P. (2018). Evaluation of artifact subspace reconstruction for automatic EEG artifact removal. *Annual International*

1074     *Conference of the IEEE Engineering in Medicine and Biology Society*, *2018*, 1242–
1075      1245. https://doi.org/10.1109/EMBC.2018.8512547

1076 Chiang, A. K., Rennie, C. J., Robinson, P. A., van Albada, S. J., & Kerr, C. C. (2011). Age
1077     trends and sex differences of alpha rhythms including split alpha peaks. *Clinical*
1078     *Neurophysiology*, *122*(8), 1505–1517. https://doi.org/10.1016/j.clinph.2011.01.040

1079 Cleeland, C., Pipingas, A., Scholey, A., & White, D. (2019). Neurochemical changes in the
1080     aging brain: A systematic review. *Neuroscience and Biobehavioral Reviews*, *98*,
1081     306–319. https://doi.org/10.1016/j.neubiorev.2019.01.003

1082 Custo, A., Van De Ville, D., Wells, W. M., Tomescu, M. I., Brunet, D., & Michel, C. M. (2017).
1083     Electroencephalographic resting-state networks: Source localization of microstates.
1084     *Brain Connectivity*, *7*(10), 671–682. https://doi.org/10.1089/brain.2016.0476

1085 Custo, A., Vulliemoz, S., Grouiller, F., Van De Ville, D., & Michel, C. (2014). EEG source
1086     imaging of brain states using spatiotemporal regression. *NeuroImage*, *96*, 106–116.
1087     https://doi.org/10.1016/j.neuroimage.2014.04.002

1088 Davis, S. W., Dennis, N. A., Daselaar, S. M., Fleck, M. S., & Cabeza, R. (2008). Que PASA?
1089     The posterior-anterior shift in aging. *Cerebral Cortex*, *18*(5), 1201–1209.
1090     https://doi.org/10.1093/cercor/bhm155

1091 Deery, H. A., Di Paolo, R., Moran, C., Egan, G. F., & Jamadar, S. D. (2023). The older adult
1092     brain is less modular, more integrated, and less efficient at rest: A systematic review
1093     of large-scale resting-state functional brain networks in aging. *Psychophysiology*,
1094     *60*(1), e14159. https://doi.org/10.1111/psyp.14159

1095 Delorme, A., & Makeig, S. (2004). EEGLAB: An open source toolbox for analysis of single-
1096     trial EEG dynamics including independent component analysis. *Journal of*
1097     *Neuroscience Methods*, *134*(1), 9–21. https://doi.org/10.1016/j.jneumeth.2003.10.009

1098 Ebitz, R. B., & Hayden, B. Y. (2021). The population doctrine in cognitive neuroscience.
1099     *Neuron*, *109*(19), 3055–3068. https://doi.org/10.1016/j.neuron.2021.07.011

1100 Férat, V., Arns, M., Deiber, M. P., Hasler, R., Perroud, N., Michel, C. M., & Ros, T. (2022).
1101     Electroencephalographic microstates as novel functional biomarkers for adult
1102     attention-deficit/hyperactivity disorder. *Biological Psychiatry. Cognitive Neuroscience*
1103     *and Neuroimaging*, *7*(8), 814–823. https://doi.org/10.1016/j.bpsc.2021.11.006

1104 Ferreira, L. K., & Busatto, G. F. (2013). Resting-state functional connectivity in normal brain
1105     aging. *Neuroscience and Biobehavioral Reviews*, *37*(3), 384–400.
1106     https://doi.org/10.1016/j.neubiorev.2013.01.017

1107 Ferreira, L. K., Regina, A. C. B., Kovacevic, N., Martin, M. da G. M., Santos, P. P., Carneiro,
1108     C. de G., Kerr, D. S., Amaro, E., Jr, McIntosh, A. R., & Busatto, G. F. (2016). Aging
1109     effects on whole-brain functional connectivity in adults free of cognitive and
1110     psychiatric disorders. *Cerebral Cortex*, *26*(9), 3851–3865.
1111     https://doi.org/10.1093/cercor/bhv190

1112 Geerligs, L., Renken, R. J., Saliasi, E., Maurits, N. M., & Lorist, M. M. (2015). A brain-wide
1113     study of age-related changes in functional connectivity. *Cerebral Cortex*, *25*(7),
1114     1987–1999. https://doi.org/10.1093/cercor/bhu012

1115 Good, C. D., Johnsrude, I. S., Ashburner, J., Henson, R. N., Friston, K. J., & Frackowiak, R.
1116     S. (2001). A voxel-based morphometric study of ageing in 465 normal adult human
1117     brains. *NeuroImage*, *14*(1 Pt 1), 21–36. https://doi.org/10.1006/nimg.2001.0786

1118 Greicius, M. (2008). Resting-state functional connectivity in neuropsychiatric disorders.
1119     *Current Opinion in Neurology*, *21*(4), 424–430.
1120     https://doi.org/10.1097/WCO.0b013e328306f2c5

1121 Gusnard, D. A., Raichle, M. E., & Raichle, M. E. (2001). Searching for a baseline: functional

imaging and the resting human brain. *Nature Reviews. Neuroscience*, *2*(10), 685–694. https://doi.org/10.1038/35094500

Hausman, H. K., O'Shea, A., Kraft, J. N., Boutzoukas, E. M., Evangelista, N. D., Van Etten, E. J., Bharadwaj, P. K., Smith, S. G., Porges, E., Hishaw, G. A., Wu, S., DeKosky, S., Alexander, G. E., Marsiske, M., Cohen, R., & Woods, A. J. (2020). The role of resting-state network functional connectivity in cognitive aging. *Frontiers in Aging Neuroscience*, *12*, 177. https://doi.org/10.3389/fnagi.2020.00177

Head, D., Buckner, R. L., Shimony, J. S., Williams, L. E., Akbudak, E., Conturo, T. E., McAvoy, M., Morris, J. C., & Snyder, A. Z. (2004). Differential vulnerability of anterior white matter in nondemented aging with minimal acceleration in dementia of the Alzheimer type: evidence from diffusion tensor imaging. *Cerebral Cortex*, *14*(4), 410–423. https://doi.org/10.1093/cercor/bhh003

Hedden, T., & Gabrieli, J. D. (2004). Insights into the ageing mind: a view from cognitive neuroscience. *Nature Reviews. Neuroscience*, *5*(2), 87–96. https://doi.org/10.1038/nrn1323

Hsu, S. H., Pion-Tonachini, L., Palmer, J., Miyakoshi, M., Makeig, S., & Jung, T. P. (2018). Modeling brain dynamic state changes with adaptive mixture independent component analysis. *NeuroImage*, *183*, 47–61. https://doi.org/10.1016/j.neuroimage.2018.08.001

Ishii, R., Canuet, L., Aoki, Y., Hata, M., Iwase, M., Ikeda, S., Nishida, K., & Ikeda, M. (2017). Healthy and pathological brain aging: From the perspective of oscillations, functional connectivity, and signal complexity. *Neuropsychobiology*, *75*(4), 151–161. https://doi.org/10.1159/000486870

Jabès, A., Klencklen, G., Ruggeri, P., Michel, C. M., Banta Lavenex, P., & Lavenex, P. (2021). Resting-state EEG microstates parallel age-related differences in allocentric spatial working memory performance. *Brain Topography*, *34*(4), 442–460. https://doi.org/10.1007/s10548-021-00835-3

Khanna, A., Pascual-Leone, A., & Farzan, F. (2014). Reliability of resting-state microstate features in electroencephalography. *PloS One*, *9*(12), e114163. https://doi.org/10.1371/journal.pone.0114163

Khanna, A., Pascual-Leone, A., Michel, C. M., & Farzan, F. (2015). Microstates in resting-state EEG: Current status and future directions. *Neuroscience and Biobehavioral Reviews*, *49*, 105–113. https://doi.org/10.1016/j.neubiorev.2014.12.010

Kirschstein, T., & Köhling, R. (2009). What is the source of the EEG. *Clinical EEG and Neuroscience*, *40*(3), 146–149. https://doi.org/10.1177/155005940904000305

Kleinert, T., Koenig, T., Nash, K., & Wascher, E. (2024). On the reliability of the EEG microstate approach. *Brain Topography*, *37*(2), 271–286. https://doi.org/10.1007/s10548-023-00982-9

Klimesch, W. (1999). EEG alpha and theta oscillations reflect cognitive and memory performance: A review and analysis. *Brain Research. Brain Research Reviews*, *29*(2–3), 169–195. https://doi.org/10.1016/s0165-0173(98)00056-3

Koenig, T., Diezig, S., Kalburgi, S. N., Antonova, E., Artoni, F., Brechet, L., Britz, J., Croce, P., Custo, A., Damborská, A., Deolindo, C., Heinrichs, M., Kleinert, T., Liang, Z., Murphy, M. M., Nash, K., Nehaniv, C., Schiller, B., Smailovic, U., … Michel, C. M. (2024). EEG-meta-microstates: Towards a more objective use of resting-state EEG microstate findings across studies. *Brain Topography*, *37*(2), 218–231. https://doi.org/10.1007/s10548-023-00993-6

Koenig, T., Prichep, L., Lehmann, D., Sosa, P. V., Braeker, E., Kleinlogel, H., Isenhart, R., & John, E. R. (2002). Millisecond by millisecond, year by year: Normative EEG

microstates and developmental stages. *NeuroImage, 16*(1), 41–48.
https://doi.org/10.1006/nimg.2002.1070

Lau, Z. J., Pham, T., Chen, S. H. A., & Makowski, D. (2022). Brain entropy, fractal
dimensions and predictability: A review of complexity measures for EEG in healthy
and neuropsychiatric populations. *The European Journal of Neuroscience, 56*(7),
5047–5069. https://doi.org/10.1111/ejn.15800

Lebel, C., Caverhill-Godkewitsch, S., & Beaulieu, C. (2010). Age-related regional variations
of the corpus callosum identified by diffusion tensor tractography. *NeuroImage, 52*(1),
20–31. https://doi.org/10.1016/j.neuroimage.2010.03.072

Li, S. C., Lindenberger, U., & Sikström, S. (2001). Aging cognition: From neuromodulation to
representation. *Trends in Cognitive Sciences, 5*(11), 479–486.
https://doi.org/10.1016/s1364-6613(00)01769-1

Lipsitz, L. A., & Goldberger, A. L. (1992). Loss of "complexity" and aging. Potential
applications of fractals and chaos theory to senescence. *JAMA, 267*(13), 1806–1809.
https://doi.org/10.1001/jama.1992.03480130122036

Liu, J., Xu, J., Zou, G., He, Y., Zou, Q., & Gao, J. H. (2020). Reliability and individual
specificity of EEG microstate characteristics. *Brain Topography, 33*(4), 438–449.
https://doi.org/10.1007/s10548-020-00777-2

Ma, M. K. H., Fong, M. C. M., Xie, C., Lee, T., Chen, G., & Wang, W. S. (2021). Regularity
and randomness in ageing: Differences in resting-state EEG complexity measured by
largest Lyapunov exponent. *Neuroimage: Reports, 1*(4), 100054.
https://doi.org/10.1016/j.ynirp.2021.100054

Mather, M. (2010). Aging and cognition. *Wiley Interdisciplinary Reviews. Cognitive Science,*
1(3), 346–362. https://doi.org/10.1002/wcs.64

McCarthy, P., Benuskova, L., & Franz, E. A. (2014). The age-related posterior-anterior shift
as revealed by voxelwise analysis of functional brain networks. *Frontiers in Aging*
Neuroscience, 6, 301. https://doi.org/10.3389/fnagi.2014.00301

Merkin, A., Sghirripa, S., Graetz, L., Smith, A. E., Hordacre, B., Harris, R., Pitcher, J.,
Semmler, J., Rogasch, N. C., & Goldsworthy, M. (2023). Do age-related differences
in aperiodic neural activity explain differences in resting EEG alpha. *Neurobiology of*
Aging, 121, 78–87. https://doi.org/10.1016/j.neurobiolaging.2022.09.003

Miall, R. C., & Robertson, E. M. (2006). Functional imaging: Is the resting brain resting.
Current Biology, 16(23), R998–R1000. https://doi.org/10.1016/j.cub.2006.10.041

Michel, C. M., & Koenig, T. (2018). EEG microstates as a tool for studying the temporal
dynamics of whole-brain neuronal networks: A review. *NeuroImage, 180 (Pt B)*, 577–
593. https://doi.org/10.1016/j.neuroimage.2017.11.062

Milz, P., Faber, P. L., Lehmann, D., Koenig, T., Kochi, K., & Pascual-Marqui, R. D. (2016).
The functional significance of EEG microstates—Associations with modalities of
thinking. *NeuroImage, 125*, 643–656.
https://doi.org/10.1016/j.neuroimage.2015.08.023

Milz, P., Pascual-Marqui, R. D., Achermann, P., Kochi, K., & Faber, P. L. (2017). The EEG
microstate topography is predominantly determined by intracortical sources in the
alpha band. *NeuroImage, 162*, 353–361.
https://doi.org/10.1016/j.neuroimage.2017.08.058

Mishra, A., Englitz, B., & Cohen, M. X. (2020). EEG microstates as a continuous
phenomenon. *NeuroImage, 208*, 116454.
https://doi.org/10.1016/j.neuroimage.2019.116454

Mullen, T. R., Kothe, C. A. E., Chi, Y. M., Ojeda, A., Kerth, T., Makeig, S., Jung, T. P., &

Cauwenberghs, G. (2015). Real-time neuroimaging and cognitive monitoring using wearable dry EEG. *IEEE Transactions on Bio-Medical Engineering*, *62*(11), 2553–2567. https://doi.org/10.1109/TBME.2015.2481482

Murray, M. M., Brunet, D., & Michel, C. M. (2008). Topographic ERP analyses: A step-by-step tutorial review. *Brain Topography*, *20*(4), 249–264. https://doi.org/10.1007/s10548-008-0054-5

Musso, F., Brinkmeyer, J., Mobascher, A., Warbrick, T., & Winterer, G. (2010). Spontaneous brain activity and EEG microstates. A novel EEG/fMRI analysis approach to explore resting-state networks. *NeuroImage*, *52*(4), 1149–1161. https://doi.org/10.1016/j.neuroimage.2010.01.093

Northoff, G., Duncan, N. W., & Hayes, D. J. (2010). The brain and its resting state activity—Experimental and methodological implications. *Progress in Neurobiology*, *92*(4), 593–600. https://doi.org/10.1016/j.pneurobio.2010.09.002

Oschwald, J., Guye, S., Liem, F., Rast, P., Willis, S., Röcke, C., Jäncke, L., Martin, M., & Mérillat, S. (2019). Brain structure and cognitive ability in healthy aging: A review on longitudinal correlated change. *Reviews in the Neurosciences*, *31*(1), 1–57. https://doi.org/10.1515/revneuro-2018-0096

Palmer, J., Kreutz-Delgado, K., & Makeig, S. (2011). AMICA: An adaptive mixture of independent component analyzers with shared components. *Swartz Center for Computational Neuroscience, University of California San Diego, Tech. Rep.* https://www.semanticscholar.org/paper/5774e96ad450c228400dc311f16caf1f20967c10

Panda, R., Bharath, R. D., Upadhyay, N., Mangalore, S., Chennu, S., & Rao, S. L. (2016). Temporal dynamics of the default mode network characterize meditation-induced alterations in consciousness. *Frontiers in Human Neuroscience*, *10*, 372. https://doi.org/10.3389/fnhum.2016.00372

Pascual-Marqui, R. D., Michel, C. M., & Lehmann, D. (1995). Segmentation of brain electrical activity into microstates: Model estimation and validation. *IEEE Transactions on Bio-Medical Engineering*, *42*(7), 658–665. https://doi.org/10.1109/10.391164

Peduzzi, P., Concato, J., Kemper, E., Holford, T. R., & Feinstein, A. R. (1996). A simulation study of the number of events per variable in logistic regression analysis. *Journal of Clinical Epidemiology*, *49*(12), 1373–1379. https://doi.org/10.1016/s0895-4356(96)00236-3

Pion-Tonachini, L., Kreutz-Delgado, K., & Makeig, S. (2019). ICLabel: An automated electroencephalographic independent component classifier, dataset, and website. *NeuroImage*, *198*, 181–197. https://doi.org/10.1016/j.neuroimage.2019.05.026

Popov, T., Tröndle, M., Baranczuk-Turska, Z., Pfeiffer, C., Haufe, S., & Langer, N. (2023). Test-retest reliability of resting-state EEG in young and older adults. *Psychophysiology*, *60*(7), e14268. https://doi.org/10.1111/psyp.14268

Poulsen, A. T., Pedroni, A., Langer, N., & Hansen, L. K. (2018). Microstate EEGlab toolbox: An introductory guide. In *bioRxiv* (p. 289850). https://doi.org/10.1101/289850

R Core Team. (2023). *R: A language and environment for statistical computing*. R Foundation for Statistical Computing, Vienna, Austria. https://www.R-project.org/

Resnick, S. M., Pham, D. L., Kraut, M. A., Zonderman, A. B., & Davatzikos, C. (2003). Longitudinal magnetic resonance imaging studies of older adults: A shrinking brain. *The Journal of Neuroscience*, *23*(8), 3295–3301. https://doi.org/10.1523/JNEUROSCI.23-08-03295.2003

Sala-Llonch, R., Bartrés-Faz, D., & Junqué, C. (2015). Reorganization of brain networks in aging: A review of functional connectivity studies. *Frontiers in Psychology*, *6*, 663. https://doi.org/10.3389/fpsyg.2015.00663

Samson, R. D., & Barnes, C. A. (2013). Impact of aging brain circuits on cognition. *The European Journal of Neuroscience*, *37*(12), 1903–1915. https://doi.org/10.1111/ejn.12183

Scally, B., Burke, M. R., Bunce, D., & Delvenne, J. F. (2018). Resting-state EEG power and connectivity are associated with alpha peak frequency slowing in healthy aging. *Neurobiology of Aging*, *71*, 149–155. https://doi.org/10.1016/j.neurobiolaging.2018.07.004

Seitzman, B. A., Abell, M., Bartley, S. C., Erickson, M. A., Bolbecker, A. R., & Hetrick, W. P. (2017). Cognitive manipulation of brain electric microstates. *NeuroImage*, *146*, 533–543. https://doi.org/10.1016/j.neuroimage.2016.10.002

Shaw, S. B., Dhindsa, K., Reilly, J. P., & Becker, S. (2019). Capturing the forest but missing the trees: Microstates inadequate for characterizing shorter-scale EEG dynamics. *Neural Computation*, *31*(11), 2177–2211. https://doi.org/10.1162/neco_a_01229

Spreng, R. N., & Turner, G. R. (2019). The shifting architecture of cognition and brain function in older adulthood. *Perspectives on Psychological Science*, *14*(4), 523–542. https://doi.org/10.1177/1745691619827511

Stevens, W. D., & Spreng, R. N. (2014). Resting-state functional connectivity MRI reveals active processes central to cognition. *Wiley Interdisciplinary Reviews. Cognitive Science*, *5*(2), 233–245. https://doi.org/10.1002/wcs.1275

Tamano, R., Ogawa, T., Katagiri, A., Cai, C., Asai, T., & Kawanabe, M. (2022). Event-related microstate dynamics represents working memory performance. *NeuroImage*, *263*, 119669. https://doi.org/10.1016/j.neuroimage.2022.119669

Tarailis, P., Koenig, T., Michel, C. M., & Griškova-Bulanova, I. (2024). The functional aspects of resting EEG microstates: A systematic review. *Brain Topography*, *37*(2), 181–217. https://doi.org/10.1007/s10548-023-00958-9

Tarailis, P., Šimkutė, D., Koenig, T., & Griškova-Bulanova, I. (2021). Relationship between spatiotemporal dynamics of the brain at rest and self-reported spontaneous thoughts: An EEG microstate approach. *Journal of Personalized Medicine*, *11*(11), 1216. https://doi.org/10.3390/jpm11111216

Tomescu, M. I., Rihs, T. A., Rochas, V., Hardmeier, M., Britz, J., Allali, G., Fuhr, P., Eliez, S., & Michel, C. M. (2018). From swing to cane: Sex differences of EEG resting-state temporal patterns during maturation and aging. *Developmental Cognitive Neuroscience*, *31*, 58–66. https://doi.org/10.1016/j.dcn.2018.04.011

Tóth, B., Kardos, Z., File, B., Boha, R., Stam, C. J., & Molnár, M. (2014). Frontal midline theta connectivity is related to efficiency of WM maintenance and is affected by aging. *Neurobiology of Learning and Memory*, *114*, 58–69. https://doi.org/10.1016/j.nlm.2014.04.009

Tröndle, M., Popov, T., Pedroni, A., Pfeiffer, C., Barańczuk-Turska, Z., & Langer, N. (2023). Decomposing age effects in EEG alpha power. *Cortex*, *161*, 116–144. https://doi.org/10.1016/j.cortex.2023.02.002

Tucker-Drob, E. M., Brandmaier, A. M., & Lindenberger, U. (2019). Coupled cognitive changes in adulthood: A meta-analysis. *Psychological Bulletin*, *145*(3), 273–301. https://doi.org/10.1037/bul0000179

Varangis, E., Habeck, C. G., Razlighi, Q. R., & Stern, Y. (2019). The effect of aging on resting state connectivity of predefined networks in the brain. *Frontiers in Aging*

Neuroscience, *11*, 234. https://doi.org/10.3389/fnagi.2019.00234

Verhaeghen, P., & Cerella, J. (2002). Aging, executive control, and attention: A review of
meta-analyses. *Neuroscience and Biobehavioral Reviews*, *26*(7), 849–857.
https://doi.org/10.1016/s0149-7634(02)00071-4

Yuan, H., Zotev, V., Phillips, R., Drevets, W. C., & Bodurka, J. (2012). Spatiotemporal
dynamics of the brain at rest—Exploring EEG microstates as electrophysiological
signatures of BOLD resting state networks. *NeuroImage*, *60*(4), 2062–2072.
https://doi.org/10.1016/j.neuroimage.2012.02.031

Zanesco, A. P. (2020). EEG electric field topography is stable during moments of high field
strength. *Brain Topography*, *33*(4), 450–460. https://doi.org/10.1007/s10548-020-
00780-7

Zanesco, A. P., King, B. G., Skwara, A. C., & Saron, C. D. (2020). Within and between-
person correlates of the temporal dynamics of resting EEG microstates. *NeuroImage*,
211, 116631. https://doi.org/10.1016/j.neuroimage.2020.116631

Zappasodi, F., Marzetti, L., Olejarczyk, E., Tecchio, F., & Pizzella, V. (2015). Age-related
changes in electroencephalographic signal complexity. *PloS One*, *10*(11), e0141995.
https://doi.org/10.1371/journal.pone.0141995

Zhang, H., Lee, A., & Qiu, A. (2017). A posterior-to-anterior shift of brain functional dynamics
in aging. *Brain Structure & Function*, *222*(8), 3665–3676.
https://doi.org/10.1007/s00429-017-1425-z

Table 1. Logistic regression results on predictors of age group by EEG microstate
transition components in Study 1.
1336

Variable	b	SE	Z (Wald)	p		OR	95% CI
(Intercept)	-1.11	0.22	-5.13	.000			
Hub C	0.11	0.19	0.60	.550		1.12	[0.78 1.61]
Hub E	1.09	0.24	4.64	.000	***	2.98	[1.88 4.73]
E-C-D rotation	-0.23	0.21	-1.09	.275		0.80	[0.53 1.20]
A-D plane	1.10	0.24	4.54	.000	***	3.01	[1.87 4.84]
B-D plane	0.83	0.24	3.51	.000	***	2.29	[1.44 3.64]
D-C-E rotation	-0.81	0.26	-3.17	.002	**	0.45	[0.27 0.73]
A-C-B rotation	0.70	0.22	3.14	.002	**	2.01	[1.30 3.11]
B-C-A rotation	-0.27	0.23	-1.19	.234		0.76	[0.49 1.19]

1337

1338 *Note. b*: coefficient for the constant in the null model; *SE*: standard error around *b*; *Z* (Wald):
1339   Wald Chi-square Statistics; OR: Odds Ratio; 95% CI: 95% confidence interval. *** *p*
1340   < .001, ** *p* < .01.

Table 2. Logistic regression results on predictors of age group by EEG microstate transition components in Study 2.

Variable	b	SE	Z (Wald)	p		OR	95% CI
(Intercept)	-0.08	0.68	-0.12	.908			
Hub C	-3.92	2.33	-1.68	.092	†	0.02	[0.00 1.91]
Hub E	0.05	0.99	0.05	.958		1.05	[0.15 7.38]
E-C-D rotation	0.93	0.99	0.94	.348		2.54	[0.36 17.79]
A-D plane	2.79	1.35	2.06	.039	*	16.21	[1.15 228.75]
B-D plane	1.55	1.03	1.51	.132		4.70	[0.63 35.24]
D-C-E rotation	-1.52	1.02	-1.48	.138		0.22	[0.03 1.63]
A-C-B rotation	0.19	0.85	0.23	.820		1.21	[0.23 6.46]
B-C-A rotation	-0.13	0.54	-0.25	.804		0.88	[0.31 2.51]

Note. b: coefficient for the constant in the null model; *SE*: standard error around *b*; *Z* (Wald): Wald Chi-square Statistics; OR: Odds Ratio; 95% CI: 95% confidence interval. * *p* < .05, † *p* < .10.

1348 **Figure Legends**

1349

Figure 1. **EEG microstate templates.**
(a) Spatial distribution of clustering maps extracted from the eye-closed resting-state data of
all 190 participants in the LEMON dataset. We selected k = 5 as the optimal number of k
according to the CV criteria. Labels A–E were assigned based on similarities with templates
identified in Asai et al. (2022) and through visual inspection based on Tarailis et al. (2024),
who unified microstate labels. (b) Example of spatial correlation between our templates and
those of other studies. We compared our templates with those of Asai et al. (2022). The spatial
correlation coefficients were computed using a vectorized 67*67 interpolated scalp map data
matrix obtained using the EEGLAB function "topoplot" to absorb differences in the number of
electrodes. In extracting microstate templates as basis vectors at this point, we ignored
topographical polarity, i.e., we only considered spatial configuration. For instance, the
topographical polarity of microstate A in Asai et al. (2022) was reversed from our microstate
A, so we aligned both maps to positive topographical polarity and then calculated their spatial
correlations for convenience. (c) We used the polarity-considered template maps. Each map
extracted by the k-means method was inverted, and a total of ten maps were used as our
microstate templates in this study. (d) The dissimilarity matrix between template maps was
defined by the spatial correlation among the five (left) or ten (right) template maps. By
subtracting the correlation coefficients from 1, we could transform a correlation matrix into a
dissimilarity matrix (one of the definitions of distance) between the topographies. These
dissimilarities range from 0 to 2; values closer to 0 indicate closer distances between two
topographies (0 means the two are the same), while values closer to 2 indicate greater
differences (2 means that the two have polarity-reversed patterns). This matrix was used to
determine the positional relationship of each template map when drawing directed graphs.

1373

Figure 2. Example of neural manifolds with spatial configurations of scalp potentials
distributed in state space using the classical multidimensional scaling method.
(a) Distribution of topography over neural state space. The method for creating neural
manifolds was based on that described by Asai et al. (2023). Each dot represented one state
of the GFP peak data (49,980 topographies collected from all 190 participants for template
clustering). The topography map was compressed into 3-D information based on spatial
dissimilarities between states and then placed on a sphere. The color of the dots indicated the
template cluster to which each state belonged (purple for microstate A, green for B, blue for
C, yellow for D, and orange for E). A large black circle in each area meant a microstate
template. The area of each template cluster comprised one square (microstate C; blue area)
and four trapezoids (microstates A, B, D, and E; purple, green, yellow, and orange areas,
respectively), which were pasted together around C to form a hemisphere, resembling a
soccer ball. In this representation, the EEG microstate templates were represented as
attractors on spherical neural manifolds. Since this was a dissimilarity-based distribution, the
same labels with different polarities (e.g., A+ and A-) were located at opposite poles of the
sphere. (b) Histogram of the vector norm for each state. Since the neural manifold was
theoretically a sphere of diameter two and radius one because it was created from
dissimilarities based on correlation coefficients (range, 0–2), a norm closer to 1 indicates that
the states are aligned on the spherical surface; thus, most of the states were located on the
sphere's surface. (c) Image of a polarity-sensitive 10-state network graph. Transitions between
template maps can be written as discrete network graphs while preserving the positional
relationships between microstate template maps in the neural state space.

1396

Figure 3. Traditional view of microstate transitions—transition probability matrices and directed graphs of microstate transition pairs ignoring topographical polarity in Study 1.

Each transition pair's average probability of occurrences was shown by placing the "from" states in the row direction and the "to" states in the column direction. Twenty transition pairs were included, except for five self-recurrences on the diagonal. In each directed graph, the nodes were the respective template maps, and the edge color indicated the transition probabilities between nodes or the magnitude of the differences between age groups. The edges of the directed graphs in (a) and (b) were only displayed if the transition probability was greater than 0.05 (= the chance level probability defined as random transitions between all states). Black squares in each transition matrix indicated transitions with valid edges in the directed graph. The distribution of nodes was defined based on the spatial correlations between templates and determined based on the dissimilarity distances compressed by classical MDS (Asai et al., 2023; Koenig et al., 2024)*. (a) Average transition probabilities for the older and (b) younger groups. (c) Differences in the average transition probabilities for each transition pair for older and younger groups. Red indicates more frequent transitions in the older group, and blue indicates less frequent transitions. (d) Standardized mean differences for comparisons between age groups (Hedge's g; Zanesco et al. (2020)). The symbol of the effect size g and red-blue colors were used to indicate the direction of the difference, with red indicating more frequent transitions and blue indicating less frequent transitions in the older group.*

Figure 4. Updated view of microstate transitions—transition probability matrices and directed graphs of microstate transition pairs when considering topographical polarity in Study 1.

Each transition pair's average probability of occurrences was shown by placing the "from" states in the row direction and the "to" states in the column direction. Ninety transition pairs were included, except for ten self-recurrences on the diagonal. In each directed graph, the nodes were the respective template maps, and the edge color indicated the transition probabilities between nodes or the magnitude of the differences between age groups. The edges of the directed graphs were only displayed if the transition probability was greater than 0.011 in (a) and (b) (≒ the chance level probability defined as random transitions between all states) and greater than 0.0011 in (c) for visualization purposes. The distribution of nodes was defined based on the spatial correlations between templates and determined based on the dissimilarity distances compressed by classical MDS (Asai et al., 2023; Koenig et al., 2024). (a) Average transition probabilities for the older and (b) younger groups. (c) Differences in the average transition probabilities for each transition pair for older and younger groups. Red indicates more frequent transitions in the older group, and blue indicates less frequent transitions. (d) Standardized mean differences for comparisons between age groups (Hedge's g; Zanesco et al. (2020)). The symbol of the effect size g and red-blue colors were used to indicate the direction of the difference, with red indicating more frequent transitions and blue indicating less frequent transitions in the older group.

Figure 5. Examples of microstate transition matrices and directed graphs for different
node definitions.
(a) Example with 14 template maps defined as nodes. (b) Addition of four template maps,
including midpoints between A-B and D-E, enabling the arrangement of template maps to
evenly divide each of the A-C-B and D-C-E axes. (c) Mean transition probabilities for each of
the older and (d) younger groups, (e) differences between the two groups, and (f) standardized
mean differences for comparisons between age groups. Details of (c)-(f) are the same as in
Figures 4a-d.

1448

Figure 6. Comparison of transition probabilities from one state to another within and
between polarities between age groups in Study 1.
(a) Schematic figure of within- and between-polarity transitions in the transition matrix. (b)
Within- and between-polarity transition probabilities by age group. The left panel shows the
probability of transitioning within polarity from each state (ABCDE±), and the right panel shows
the probability of transitioning between polarities from each state.

1455
Note. *** adjusted *p* (adj.*p*) < .001, ** adj.*p* < .01, * adj.*p* < .05, † adj.*p* < .10. Error bars
indicated the standard errors.

Figure 7. Inter-participant correlation matrix between the number of transitions between
EEG microstate templates in Study 1.
We divided the EEG topographical dynamics into 100 distinct transitions by applying ten
polarity-sensitive EEG microstate templates. Correlations between transition pairs were then
calculated based on the number of transitions counted from each participant's EEG data. The
rows and columns were sorted according to the results of Varimax-rotated PCA, in order of
absolute loading values, for each of the eight components formed by collecting the items with
the highest (most contributing) absolute loading values. Dotted delimiters indicated the
boundaries of the components. Each of the eight blocks of diagonal components surrounded
by dotted lines corresponded to eight transition components found in the rotated PCA. For
simplicity in the axis labels in the figure, positive polarity templates were denoted by uppercase
letters (A, B, C, D, E) and negative polarity templates by lowercase letters (a, b, c, d, e), in
"transition from" state/"transition to" state order (e.g., "Ab" label meant the transition from A+
to B-).

1472

Figure 8. Principal component analysis for EEG microstate transition signatures in Study 1.

(a) Parallel analysis scree plot to determine the number of principal components (PCs). The blue line indicated PC eigenvalues obtained from the actual data, and the red dotted lines indicated that they were estimated from simulated/resampled data. Parallel analysis suggested that eight components were the optimal number of PCs. (b) Graph of cumulative contribution ratio as a function of the number of PCs. The eight PCs selected based on the parallel analysis suggestions explained 87.65% of the data variance. (c) List of transition pairs contributing to each PC. After Varimax rotation of the eight principal component axes resulting from the PCA for interpretation, each transition pair was assigned to the component with the highest absolute rotated component loadings. See Supplementary materials (Table S1) for the complete rotated component loading matrix.

1485

Figure 9. Transition component scores for each age group in Study 1.
The green bar shows the transition component scores for the younger group, while the orange
bar shows those for the older group. Transition components with mostly negative contributing
transition pairs were inverted. Hence, a higher transition component score signifies a
pronounced trend in that specific transition component, i.e., the transition probability of the
contributing transition pairs tends to be high. Conversely, a lower score indicates the opposite.

1492
Note. *** adjusted *p* (adj.*p*) < .001, ** adj.*p* < .01, * adj.*p* < .05, † adj.*p* < .10. Error bars
indicated the standard errors.

Figure 10. Updated view of microstate transitions—transition probability matrices and
directed graphs of microstate transition pairs when considering topographical polarity
in Study 2.
Each transition pair's average probability of occurrences was shown by placing the "from"
states in the row direction and the "to" states in the column direction. Ninety transition pairs
were included, except for ten self-recurrences on the diagonal. In each directed graph, the
nodes were the respective template maps, and the edge color indicated the transition
probabilities between nodes or the magnitude of the differences between age groups. The
edges of the directed graphs were only displayed if the transition probability was greater than
0.011 in (a) and (b) (≐ the chance level probability defined as random transitions between all
states) and greater than 0.0011 in (c) for visualization purposes. (a) Average transition
probabilities for the older and (b) younger groups. (c) Differences in the average transition
probabilities for each transition pair for older and younger groups. Red indicates more frequent
transitions in the older group, and blue indicates less frequent transitions. (d) Standardized
mean differences for comparisons between age groups (Hedge's g; Zanesco et al. (2020)).
The symbol of the effect size g and red-blue colors were used to indicate the direction of the
difference, with red indicating more frequent transitions and blue indicating less frequent
transitions in the older group.

1513

1514 **Figure 11. Comparison of transition probabilities from one state to another within and**
1515 **between polarities between age groups in Study 2.**
1516 *The left panel shows the probability of transitioning within polarity from each state (ABCDE±),*
1517 *and the right panel shows the probability of transitioning between polarities from each state.*

1518
1519 *Note.* *** $p < .001$, ** $p < .01$, * $p < .05$, † $p < .10$. Error bars indicated the standard
1520 errors.

Figure 12. Confirmation of the structure of co-occurrence transitions in Study 2.
(a) Graph of cumulative contribution ratio as a function of the number of PCs when applying the eigenvectors and rotation matrix obtained in Study 1 to independent data in Study 2. The eight PCs explained 78.29% of the data variance. (b) List of transition pairs contributing to each PC. After applying the eigenvectors and Varimax rotation matrix in Study 1 to Study 2, each transition pair was assigned to the component with the highest absolute rotated component loadings. Subsequently, we replicated the eight principal component axes. See Supplementary materials (Table S2) for the complete rotated component loading matrix.

Figure 13. Transition component scores for each age group in Study 2.
The green bar shows the transition component scores for the younger group, while the orange
bar shows those for the older group. Transition components with mostly negative contributing
transition pairs were inverted. Hence, a higher transition component score signifies a
pronounced trend in that specific transition component, i.e., the transition probability of the
contributing transition pairs tends to be high. Conversely, a lower score indicates the opposite.

1536
1537 *Note.* * $p < .05$, † $p < .10$, *ns*.: no significance. Error bars indicated the standard errors.