Photoreceptor loss does not recruit neutrophils despite strong microglial activation

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Impact statement: Systemic neutrophils do not respond to laser-induced photoreceptor damage despite the robust response from resident microglia

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Data availability statement: All data collected (~3 TB) is archived at the University of Rochester and is available upon request.

Abstract:

In response to central nervous system (CNS) injury, tissue resident immune cells such as microglia and circulating systemic neutrophils are often first responders. The degree to which these cells interact in response to CNS damage is poorly understood, and even less so, in the neural retina which poses a challenge for high resolution imaging in vivo. In this study, we deploy fluorescence adaptive optics scanning light ophthalmoscopy (AOSLO) to study fluorescent microglia and neutrophils in mice. We simultaneously track immune cell dynamics using label-free phase-contrast AOSLO at micron-level resolution. Retinal lesions were induced with 488 nm light focused onto photoreceptor (PR) outer segments. These lesions focally ablated PRs, with minimal collateral damage to cells above and below the plane of focus. We used in vivo (AOSLO, SLO and OCT) imaging to reveal the natural history of the microglial and neutrophil response from minutes-to-months after injury. While microglia showed dynamic and progressive immune response with cells migrating into the injury locus within 1-day after injury, neutrophils were not recruited despite close proximity to vessels carrying neutrophils only microns away. Post-mortem confocal microscopy confirmed in vivo findings. This work illustrates that microglial activation does not recruit neutrophils in response to acute, focal loss of photoreceptors, a condition encountered in many retinal diseases.

Introduction

In the mammalian retina, a rapid and coordinated immune response to infection

or injury is important for maintaining tissue homeostasis. This is especially critical

in the eye since mature retinal neurons do not typically regenerate, resulting in

long-term functional losses for the host.[1,2] The retina is considered immune-

privileged and is equipped with a resident population of innate immune cells

including microglia.[3,4] Under homeostatic conditions, microglia are distributed

primarily in the inner retina, residing within nerve fiber layer (NFL), inner

plexiform layer (IPL) and outer plexiform layers (OPL).[5,6], generally avoiding the

nuclear layers of the retina. Microglia tile the retina and like their counterparts in

the brain, exhibit long, thin cellular processes that continually probe the neuro-

glial microenvironment.[4,7,8]

In addition to phagocytosing debris[9,10], regulating synaptic

maintenance[11,12] and removing dead tissue[13,14], microglia can secrete

chemokines to recruit other leukocytes to help fight infection and repair damaged

tissue.[4,15–17] For a number of injuries, one of the first systemic responders

recruited and activated by microglia are neutrophils.[18,19] Neutrophils comprise a

large fraction of leukocytes in murine blood (7.4 – 33.9%, "young" C57BL/6J

mice[20]). They assist in maintaining tissue homeostasis by neutralizing foreign

agents, regulating the immune response, and processing dead tissue via

phagocytosis[21,22]. Beyond these well-known functions, they are also implicated

in becoming activated in conditions of shock and trauma[23]. Under inflammatory

conditions, the spatiotemporal interplay between microglia and neutrophils is

poorly understood. A missed window of interaction is highly problematic in

histological study where a single time point only reveals a snapshot of the

temporally complex immune response, which changes dynamically over time.

Here, we use in vivo imaging to overcome these constraints.

Documenting interactions between immune cells in the retina over time

has been challenged by insufficient resolution and contrast to visualize single

immune cells in the living eye. Recently, advances in AOSLO imaging have

provided micron-level resolution and enhanced contrast for imaging individual

immune cells in the retina[7,24], and do so without requiring extrinsic dyes. This is

achieved by using near infrared (NIR) light, to which the eye is less sensitive, and

combining this with phase-contrast approaches[25–27]. In addition, AOSLO

provides multi-modal information from confocal reflectance, phase-contrast and

fluorescence modalities, which can reveal a variety of cell types simultaneously

in the living eye. Here, we used confocal AOSLO (<6 μm axial resolution[28,29]) to

track changes in reflectance at cellular scale. Phase-contrast AOSLO provides

detail on vascular wall, single blood cells[30–32], PR somata[33], highly translucent

retinal cells, and is particularly suited to image resident and systemic immune

cells.[7,24] Simultaneous fluorescence imaging provides the ability to study

fluorescently-labeled cells[26,29,34] and exogenous dyes[30,35] throughout the living

retina. These modalities used in combination have recently provided detailed

images of the retinal response to a model of human uveitis.[24,36] Together, these

innovations now provide a platform to visualize, for the first time, the dynamic

interplay between many immune cell types, each with a unique role in tissue

inflammation. We combine these innovative modalities with conventional

histology as well as commercial OCT to reveal the progressive nature of the

cellular response to acute retinal injury.

As this work is in its early inception, we focus on one of many immune cell

interactions, the interplay of two critical first responders to injury: neutrophils and

microglia. To begin unraveling the complexities in this response, we examine the

innate immune response to a deep retinal laser ablation model. Using AOSLO,

we track and characterize the spatial, axial and temporal changes in microglia,

neutrophils and retinal structure within hours, days and months after acute laser

exposure.

Methods:

Key Resources Table				
Reagent type (species) or resource	**Designation**	**Source or reference**	**Identifiers**	**Additional information**
strain, strain background (*Mus musculus*)	C57BL/6J	The Jackson Laboratory	Strain #: 000664	
strain, strain background (*Mus musculus*)	CX3CR1-GFP	The Jackson Laboratory	Strain #: 005582	
strain, strain background (*Mus musculus*)	Catchup	Laboratory of M. Gunzer	C57BL/6-*Ly6g*(tm2621(CretdTomato)Arte	(Hasenberg *et al.* 2015) [37]
antibody	Ly-6G-647	Biolegend	Cat #: 127610 RRID:AB_1134159	IF (1:200)

other	DAPI stain	Cell Signaling Technology	Cat #: 4083	1:500 of 10 mg/ml stock
chemical compound, drug	Lipopolysaccharide (LPS)	Sigma-Aldrich	Cat #: L4391	1 ng (1 μl) delivered intravitreally
software, algorithm	Cell counter plugin	Imagej FIJI	Cell counter plugin	Author: Kurt De Vos, Imagej version 1.53q

Mice

All experiments herein were approved by the University Committee on Animal

Resources (protocol #: UCAR-2010-052E) and according to the Association for

Research in Vision and Ophthalmology statement for the Use of Animals in

Ophthalmic and Vision Research as well as institutional approvals by the

University of Rochester. C57BL/6J (#000664, Jackson Labs, Bar Harbor, ME)

mice were used to track the retinal phenotype after laser exposure.

Heterozygous CX3CR1-GFP (#005582, Jackson Labs) mice were used to track

GFP-expressing microglia. Mice with heterozygous transgenic expression of

tdTomato in neutrophils ("Catchup" mice) were provided by the foundry lab of M.

Gunzer.[37] 18 mice (10 male, 8 female) in total were used for *in vivo* imaging. 10

additional mice (5 male, 5 female) were used for *ex vivo* histology. Age for all

mice used for this work were between post-natal weeks 6 - 24.

Preparation for *in vivo* imaging

Mice were anesthetized with intra-perotineal injection of ketamine (100 mg/kg)

and xylazine (10 mg/kg). The pupil was dilated with 1% tropicamide (Sandoz,

Basel, Switzerland) and 2.5% phenylephrine (Akorn, Lake Forest, IL). A custom

contact lens (1.5 mm base curve, 3.2 mm diameter, +10 diopter power,

Advanced Vision Technologies, Lakewood, CO) was fitted to the eye. For a

subset of experiments, 50 mg/kg fluorescein (AK-FLUOR, Akorn, Decatur, IL)

was administered by intra-perotineal injection to confirm vascular integrity and

perfusion status after injury. During AOSLO imaging, anesthesia was

supplemented with 1% (v/v) isoflurane in oxygen and mice were maintained at

37°C via electric heat pad. Eye hydration was maintained throughout imaging

with regular application of saline eye drops (Refresh tears, Allergan, Sydney,

Australia) and lubricating eye gel (Genteal, Alcon Laboratories Inc. Fort Worth,

TX) in combination with rigid contact lens described above. Mice were placed in

a positioning frame with 6-degrees of freedom to allow for stable animal

positioning and to aid in retinal navigation relative to the beam of the AOSLO and

OCT.

***In vivo* AOSLO imaging**

Four light sources were used for AOSLO imaging. A 904 nm diode source (12

μW, Qphotonics, Ann Harbor, MI) was used for wavefront sensing. A second

796 nm superluminescent diode (196 μW, Superlum, Cork, Ireland) was used for

reflectance imaging, including confocal and phase contrast modes.[29,30] A third

488 nm light source (56 μW, Toptica Photonics, Farmington, NY) was used to

visualize GFP-positive microglia in CX3CR1-GFP mice. A fourth 561 nm light

source (95 μW, Toptica Photonics) was used to visualize tdTomato-positive

neutrophils in Catchup mice. All light sources were fiber-coupled and were axially

combined through the AOSLO system in a free-space design[29]. Fast (15.4 kHz)

and slow (25 Hz) scanners create a raster scan pattern, which is relayed through

a series of afocal telescopes to and from the eye. A Shack-Hartmann wavefront

sensor (consisting of a lenslet array and a Rolera XR camera, QImaging, Surrey,

Canada) measures the aberrations of the eye and a 97 actuator deformable

mirror (ALPAO, Montbonnot-Saint-Martin, France) provided the wavefront

correction. Reflected 796 nm light was collected with a photomultiplier tube

(H7422-50, Hamamatsu Photonics, Hamamatsu, Japan). All confocal reflectance

images were captured with a 30 μm pinhole (1.3 Airy Disc Diameters, ADD).

Phase-contrast was achieved by displacing the pinhole relative to the principal

axis of the detection plane as previously described.[26] Fluorescence was captured

with a photomultiplier tube (H7422-40, Hamamatsu) either coupled with a

520Δ35 band-pass filter (FF01-520/35-25, Semrock, Rochester, NY) for GFP

emission, or a 630Δ92 band-pass filter (FF01-630/92-25, Semrock) for tdTomato

emission. All fluorescent images were captured with a confocal 50 µm pinhole

(2.1 ADD). Image field sizes were either 4.98° x 3.95° or 2.39° x 1.94°. NIR and

visible imaging channels were made coplanar, compensating for longitudinal

chromatic aberration by independently focusing each light source so it projected

onto the same axial structure in the retina. Through-focus acquisitions were

acquired by sequentially changing the focus from nerve fiber layer through to the

PR outer segments by using the defocus term on the custom adaptive optics

control software. This strategy allowed depth imaging while keeping all visible

and NIR sources conjugate to the same axial plane.

As described previously, red blood cell (RBC) imaging was achieved by

combining phase-contrast imaging with a strategy to arrest the slow

galvanometer scanner and let the resonant scanner project a single "line" on the

retina. This enabled RBC flux imaging by positioning this line orthogonal to the

direction of flow for single capillaries. As blood cells moved through capillaries,

they were "self-scanned" producing images of RBCs in space/time images[30]

(Figure 4 – figure supplement 1b + f). Scan angle for this modality was 0.71°.

PR laser damage model and post-injury time points for imaging

488 nm light (Continuous wave Laser diode, ±4 nm bandwidth, Toptica

Photonics) was used to create an acute laser injury. Laser light was projected

through the AOSLO and focused onto the PR outer segments. To create

damage, 785 µW of 488 nm light was focused onto the PR outer segments for 3

minutes in a single line on the retina subtending 24 x 1 µm to concentrate the

power to a small focal region. Laser injuries were placed between 5-15° from the

optic disc. To avoid absorption confounds, we avoided placing lesions beneath

large retinal vessels. For experiments examining neutrophil involvement, lesions

were placed less than ~100 microns away from retinal veins and within microns

of capillaries to increase the chance of extravasation through these preferred

pathways in the retina[38–40]. As many as four such lesions were placed per retina

(Figure 1). We chose to use the above protocol as an established way to create

modest, consistent and reproducible outer retinal damage.

Throughout this work, we assessed the effects of the laser injury for the

following time points: baseline/control, 1 day (defined as 18 – 28 hours post-

damage), 3 days, 7 days and 2 months.

***In vivo* SLO, and OCT imaging**

To confirm global ocular health and changes imparted by the laser damage, a

commercial Heidelberg Spectralis system (Heidelberg, Germany) was used to

acquire scanning laser ophthalmoscopy (SLO) and optical coherence

tomography (OCT) images. 30° and 55° fields were used for SLO acquisitions.

The 30° field was used for OCT acquisitions. The wider imaging fields allowed for

global views not only of damage locations, but also adjacent, non-damaged

retina. For some experiments, fluorescein angiography was captured by imaging

the retina within 10 minutes of fluorescein administration (details above). As an

additional advantage, the fluorescence mode of the Spectralis enabled wide-field

images of GFP positive microglia (Figure 5a, right).

OCT was acquired with the following settings: ART 16 (automatic real-time

tracking) was used to average B-scans to improve signal. To capture several

damage locations in a single field, we used a coarse scan area (61 B-scans over

a 1.02 x 0.85 mm window, Figure 1c). A dense 3D data cube was also captured

(513 x 171 µm, 49 progressive B-scans, Figure 2a) to provide the most detailed

information regarding the axial nature of the laser damage. "Follow-up" mode,

which allows HRA software to return to the same retinal location, was used

whenever possible. To reveal the cross-sectional profile for each lesion, several

adjacent B-scans were spatially averaged (~30 µm).

Preparation for *ex vivo* imaging

Mice were euthanized by CO_2 asphyxiation followed by rapid cervical dislocation.

Eyes were enucleated and placed in 4% paraformaldehyde (PFA, diluted from:

#15714-S, Electron Microscopy Sciences, Hatfield, Pennsylvania) in 1x

phosphate buffered saline (PBS, #806552, Sigma-Aldrich, St. Louis, MO) within 5

minutes of asphyxiation. Intact eye globes were left in PFA fix for one hour at

room temperature. Eyes were dissected to remove the cornea, lens and vitreous.

Each eye cup was placed in one well of a 24-well plate containing 0.5 ml of 0.8%

PFA and left overnight at 4°C. The retina was separated from the retinal

pigmented epithelium/choroid with attention to preserve inner retinal layers "up"

orientation. If not applying antibody, the tissue was directly flat mounted (see

below). For antibody staining, the retina was placed in 1x BD perm/wash buffer

(#554723, BD Biosciences, Franklin Lakes, NJ) with 5% donkey serum (#D9663,

Sigma-Aldrich) diluted in PBS for overnight incubation at room temperature with

gentle shaking. The following was performed in the dark. Ly-6G-647 antibody

(1:200, #127610, RRID:AB_1134159, BioLegend, San Diego, CA) and DAPI

(1:500 of 10 mg/ml stock, #4083, Cell Signaling Technology, Danvers, MA) were

diluted in 1x perm/wash buffer and retinas were incubated for 3 days at room

temperature with gentle shaking. Retinas were washed with PBS three times

over three hours. The retina was cut into 4 radially symmetrical petals, flat-

mounted on a glass slide in ~40 µl of Vectashield mounting buffer (H-1000-10,

Vector labs, Newark, CA) with a #1.5 cover slip (#260406, Ted Pella Inc.,

Redding, CA), sealed with nail polish and stored at 4°C until imaged.

Endotoxin-Induced Uveitis protocol

To serve as a positive control and show evidence of known neutrophil invasion,

we adopted the endotoxin-induced uveitis model to confirm that fluorescent

neutrophils could be observed in vivo with AOSLO. This was performed in two

mice. The endotoxin-induced uveitis model has been described previously.[36,41]

Briefly, we performed intravitreal injections of lipopolysaccharide (LPS, #L4391,

Sigma-Aldrich). Mice were anesthetized with ketamine and xylazine. A 34 gauge

Hamilton needle was used to deliver 1 µL (1 ng) of LPS diluted in PBS into the

vitreous space posterior to the limbus. 1 day post-LPS injection, mice were either

imaged with AOSLO (Catchup mice) or collected for *ex vivo* histology (Ly-6G-647

stained C57BL/6J mice) to confirm fluorescent neutrophil presence in the neural

parenchyma.

***Ex vivo* confocal imaging**

Whole-mount retinas were imaged with a Nikon A1 confocal microscope

(Melville, NY). DAPI (405 nm ex, 441Δ66 nm em), CX3CR1-GFP (488 nm ex,

525Δ50 nm em), and Catchup/anti-Ly-6G-647 (635 nm ex, 665Δ50 nm em) were

simultaneously imaged. Z-stacks at control or laser-damaged locations were

acquired with a 60x oil objective, producing images that were 295 x 295 µm. Z-

stack axial sectioning was performed with either 0.1 or 0.5 µm step size. Larger

(796 x 796 µm) 60x z-stacks were acquired by blending several 60x z-stack

acquisitions (3x3, 15% overlap) using the native Nikon NIS Elements software.

AOSLO image processing

To correct for residual motion from heart rate and respiration, AOSLO images

were registered with a custom cross-correlation-based frame registration

software.[42,43] Motion correction was also applied to simultaneously collected

fluorescence images. After registration, confocal, phase-contrast and

fluorescence AOSLO images were temporally averaged (250 frames, 10

seconds). Blood perfusion maps were computed by calculating the standard

deviation of pixel intensity over 30 seconds[34] (Figure 4).

***Ex vivo* confocal image processing**

Imagej FIJI (free NIH software)[44] was used to view and manage data files.

Confocal z-stacks were re-sliced (X-Z dimension) to visualize fluorescence depth

profiles.

INL + ONL nuclei quantification

Raw DAPI z-stacks were used for manual counting of nuclei (n = 10 mice, 3

unique regions per time point). Analysis regions were circular, with a 50 μm

diameter (roughly corresponding to the size and shape of the damage region

seen with confocal AOSLO, Figure 3e) and analyzed in depth producing

volumetric cylinders through the INL or outer nuclear layer (ONL, Figure 3d).

Nuclei were counted manually using the "Cell Counter" plugin in Imagej (Author:

Kurt De Vos, Imagej version 1.53q).

PR + Microglia nuclei volume quantification

A single DAPI-stained z-stack (OPL + ONL) from a CX3CR1-GFP mouse was

used to quantify nuclear volume of PR's (n = 20) and microglia (n = 14). Data

was centered at a lesion location 3 days post-laser exposure. Imagej was used to

manually measure the en-face diameter of nuclei in their short and long axis. We

averaged the two measurements and assumed spherical shape for analysis.

These measurements aided in the differentiation of PR's, invading microglia and

PR phagosomes.

Quantification of RBC flux in capillaries

Using the line-scan approach across single capillaries[30,45,46], we quantified RBC

flux within an epoch of 1 second. This spanned several cardiac cycles.[32,47] To

improve SNR, space-time images were convolved with a Gaussian spatio-

temporal filter (σ = 7.5 pixels, 0.33 μm). This strategy did not interfere with

spatial resolution as pixels oversample the optical point-spread of the AOSLO by

>20x.[30] RBC flux was determined by manually marking blood cells using the "Cell

counter" plugin in Imagej.

Neutrophil density quantification

Ly-6G-647-stained retinal tissue was used to manually count neutrophils within

montaged 796 x 796 μm z-stacks. Cells were counted at control (n = 4 locations,

2 mice) and lesioned (n = 4 locations, 2 mice) locations using the "Cell Counter"

Imagej plugin. All values are reported as mean ± SD. There were no data points

omitted from any of the analysis reported in this work.

Results:

Characterization of deep focal laser damage

Four complementary imaging modalities were used to evaluate the nature and

localization of the focal laser damage induced by 488 nm light: wide field SLO,

OCT, AOSLO and post-mortem histology. Each is reported in turn below.

Laser damage induces focal hyperreflective lesions in outer retina imaged

with wide-field SLO

To observe global and focal retinal health, we used commercial SLO. 1 day post-

488 nm light exposure, both NIR and blue reflectance modalities showed

hyperreflective lesions, most apparent at a deeper retinal focus position. When

SLO focus was brought to the inner retina, lesions were not visible and retina

appeared otherwise healthy (Figure 1b). Despite the deep retinal damage

phenotype, fluorescein angiography did not reveal dye leakage (Figure 1b,

bottom), indicating the blood retinal barrier remained intact.

OCT B-scans reveal outer retinal hyperreflection without inner retinal

damage

To assist in determination of which retinal layers are damaged by the 488 nm

laser, we used OCT. Within 30 minutes post-laser exposure, OCT revealed a

zone of hyperreflection within the ONL (Figure 2 – figure supplement 1). 1 day

post-lesion, the focal hyperreflection remained localized to the ONL (~50 microns

wide, Figure 1c, 2a). With OCT, the retina laterally adjacent to damage foci

appeared normal. The hyperreflective phenotype persisted through 7 days post-

damage and was cleared by 2 months (Figure 2a). There did not appear to be

any cellular excavation, "cratering" or evidence of edema for any post-exposure

time point assessed. Despite the axially localized hyperreflective phenotype,

Bruch's membrane appeared intact for all time points assessed. This was

evidenced by lack of fluorescein leakage at the site of lesion. Additionally, retinal

vessels appeared normal in OCT B-scans aligning with findings from fluorescein

angiography, vascular perfusion and histology (discussed below).

AOSLO reveals outer retinal damage with confocal and phase-contrast modalities

Confocal AOSLO provided micron-level detail of the lesioned area. Confirming OCT findings, we observed hyperreflective changes localized within the ONL that were, by 1 day, the brightest at the OPL/ONL interface, shown in Figure 2b. The AOSLO has an axial resolution near 6 μm[29] and thus evidence of retinal capillaries at the deepest vascular stratification acted as an axial landmark for the OPL. At this plane, the lesions manifest as an elliptical region with the long axis in the direction of the linescan used to create the lesion. Tracking this region over time, showed most prominent hyperreflectivity at 1 day post lesion, with diminishing size and brightness by day 3 and 7. The hyperreflective phenotype was largely diminished by 2 months post-exposure (Figure 2b).

Using phase-contrast AOSLO also allowed visualization of translucent cells within the retina which enabled us to image PR somas of the ONL[26,33]. Normally, the ONL is comprised of 8-12 PR somata that are axially stacked[33,48]. We found that the dense packing of individual somata was disrupted 1 day post-exposure (~50 μm ovoid, Figure 2c), suggesting degradation or ablation of the cell membrane.

Confirmation of outer retinal cell loss using post-mortem histology

To assess the extent of cell loss caused by focal laser exposure, we performed DAPI staining on whole-mount retinal tissue using the same time points

assessed previously for *in vivo* imaging. 1 day after laser exposure, we observed

mild thickening of the ONL compared to unexposed locations only microns away.

At 3 and 7 days, local ONL thinning was observed (Figure 3a). En-face planes at

multiple layers within the ONL revealed a loss of PR nuclei in the outer aspect of

the ONL for 3 and 7 day time points (Figure 3c). The inner ONL exhibited little

evidence of cell loss (Figure 3b), illustrating the precise axial confinement of the

laser damage being induced by this method. By 2 months, the lesion's overall

appearance and ONL thickness returned to baseline (Figure 3a-c). This

histological finding corroborates the OCT findings observed *in vivo*.

ONL nuclear counts were reduced at locations of laser exposure. In

comparison to control locations (501317 nuclei/mm^2 ± 46198 nuclei/mm^2, mean

±SD, similar to previous work[49]), at 3 and 7 days post-exposure, we found a

corresponding reduction in the density of ONL nuclei of 18% (408965 nuclei/mm^2

± 25621 nuclei/mm^2) and 27% (367542 nuclei/mm^2 ± 9038 nuclei/mm^2)

respectively. Calculated in comparison to control locations, the 3 and 7 day data

resulted in p-values of 0.17 and 0.07, respectively (Student's, paired two-tailed, t-

test). 2 months after damage, PR nuclear densities were indistinguishable from

that of control (Figure 3f, gray bars). Despite losses of PR nuclei, total cell nuclei

within the INL remained unchanged for all time points (Figure 3f, black bars).

These data indicate that the laser exposure focally ablated PR's whilst leaving

inner retinal cells intact.

Retinal vasculature unaffected by deep retinal lesion

A concern with laser lesions of this type is that it may coagulate large vessels or

capillaries. Motion contrast[27,30] images revealed that the vasculature remained

perfused from hours to months after laser damage suggesting that acute or long

term changes are not imparted by the laser injury (Figure 4). None of the primary

vascular stratifications within the NFL, IPL and OPL of the mouse retina[34]

showed stopped flow as a result of the laser lesion, reinforcing the findings above

regarding the axial confinement of the damage to the outer retina.

In addition to perfusion status, phase-contrast AOSLO also permitted

analysis of single blood cell flux within capillaries[30,50]. We tracked capillary flux at

different retinal depths within and above damage sites (IPL, OPL, 1 capillary

each, Figure 4 – figure supplement 1a). Blood cell flux for capillaries within lesion

locations were within the range of normal flux for the C57BL/6J mouse[50] (Figure

4 – figure supplement 2b, c). Flux tracked from hours to days in these capillaries

changed synchronously, displaying positive linear correlation (R^2 = 0.59, Figure 4

– figure supplement 1c, d). This suggested any such changes in flux were a

property of systemic perfusion, rather than locally imparted changes in flow due

to the lesion. As an additional control, we evaluated blood flux in two distant

capillaries; one located 10-15° temporal of the optic disc (lesion location) and

another of equivalent eccentricity on the nasal side (control, Figure 4 – figure

supplement 1e). Both capillaries displayed similar flux values from minutes to 2

months post-injury (Figure 4 – figure supplement 1f, g) resulting in positive linear

correlation (R^2 = 0.78, Figure 4 – figure supplement 1h). Taken together, these

findings suggest lesions do not rupture or stall blood flow in capillaries, nor do

they appreciably impact total RBC delivery in the capillary network.

PR laser injury promotes a robust response in nearby microglia

To observe the microglial response to PR laser injury, we imaged fluorescent

microglia in CX3CR1-GFP mice with both SLO and AOSLO. 1 day after injury,

SLO revealed bright, focal congregations of microglia at injury locations. This

was in contrast to undamaged locations which maintained a distribution

resembling lateral tiling (Figure 5a, b). The global visualization of microglia was

augmented by high resolution fluorescence AOSLO, providing enhanced detail of

the microglial response to laser injury, especially cellular process detail[7,51].

Whereas AOSLO imaging of microglia in the healthy retina displayed a

distributed array of microglia with ramified processes (Figure 5c, left), laser

damaged locations showed a congregation of cells 1 day post-injury with less

lateral ramification (Figure 5c, right). Within hours of the laser exposure, we did

not observe a photo-bleaching or death of regional microglia suggesting that

while the laser exposure was sufficient to damage PR's, it left inner retinal

microglia intact.

A standing question in OCT/confocal AOSLO interpretation is whether

microglia contribute or directly produce the hyperreflective phenotype seen in

axial B-scans and en-face fundus images[52,53]. With confocal AOSLO, we find

that the hyperreflective phenotype is visible as early as 30 minutes and becomes

slightly larger and brighter by 90 minutes. During these time points,

simultaneously imaged microglia remained ramified and maintained a tiled

arrangement, indicating that microglial are not the initial source of the lesion-

induced hyperreflective appearance (Figure 6 – figure supplement 1).

We returned to the same laser-damaged locations to capture microglial

appearance at baseline, 1, 3, 7 day and 2 month time points with AOSLO to track

the natural history of the microglial response to PR damage. At 1 day post-injury,

damage locations displayed aggregations of microglia. The surrounding microglia

displayed process polarization with extensions projecting toward the injury

(Figure 6). By days 3 and 7, microglia exhibited fewer lateral projections and

somas have migrated into the ONL where they do not normally reside (Figure 6).

By 2 months post-injury, the hyperreflective phenotype was absent and microglia

once again occupied only the inner retina. The axial and lateral microglial

distribution at 2 months after lesion was similar to baseline (Figure 6).

Additionally, cell morphology once again showed radially symmetrical branching

projections, similar to those prior to laser injury.

With phase-contrast imaging targeting the ONL, we documented a rare

event of putative pseudopod extension at a lesion site (Figure 5 – video 1). Given

the axial complexity of microglia in this layer (Figure 9 – figure supplement 2c) it

is now possible that microglial process dynamics may be revealed with this label-

free approach.

Despite robust microglial involvement, neutrophils do not extravasate

While we observed a robust microglial response to PR damage, there was no evidence of neutrophil involvement at the times we examined (1, 3, 7 day, and 2 month follow-up).

In vivo fluorescence imaging allowed us to track neutrophils with AOSLO in "Catchup" mice[37]. In healthy mice, we observed a sparse population of circulating neutrophils flowing quickly within the largest retinal vessels (Figure 7 – video 1). We also observed neutrophils moving through single capillary branches (Figure 7 – video 2). This provided evidence that neutrophils could be directly observed in vivo, where they are moving at exceptionally fast speed[32]. Within capillaries, we found that neutrophils show deformation within the small confines of the capillary lumen, often resulting in tube or pill-shaped neutrophil morphology seen both in vivo and ex vivo (Figure 7b, top).

After inducing laser lesion, we found no evidence of neutrophil aggregation or extravasation for any time point assessed (Figure 8). There was also a notable lack of rolling/crawling neutrophils (or any putative leukocyte) in large arterioles or venules surrounding the injury (Figure 8 – video 1). The deepest retinal neutrophils, closest to the ONL lesion, were occasionally detected within the deepest retinal capillaries. However, these neutrophils stayed within the retinal vasculature, as evidenced by their pill-shaped morphology and passage routes that follow the known vascular paths seen in confocal/phase

contrast imaging (Figure 8 – video 2). Just like healthy mice, leukocytes,

including neutrophils often impede flow due to their large size (13.7 μm[54]) as they

must compress through capillaries <7 μm in diameter[50]. However, we found no

evidence of permanently stopped flow, as the rare stalls would re-perfuse similar

to those previously characterized in healthy mice (Figure 7a).[50]

As a positive control, we used the endotoxin-induced uveitis model in

Catchup mice to show evidence that we could image extravasated neutrophils.

This model is known to induce a strong neutrophil response. With fluorescence

AOSLO, we found aggregation of Catchup-positive neutrophils within the retinal

parenchyma, providing confirmation that extravasated neutrophils can be imaged

with this modality. Moreover, we found that neutrophils that have extravasated

into the retinal parenchyma tended to have a more spherical morphology rather

than the compressed, pill-shaped morphology of neutrophils within capillaries

(Video 2).

***Ex vivo* analysis confirms *in vivo* findings**

To confirm our *in vivo* findings and make certain that no neutrophils evaded

detection with *in vivo* imaging, we examined fluorescent microglia and

neutrophils in laser-damaged retinal whole-mounts imaged with confocal

microscopy. Both the spatial and progressive nature of the microglial response to

PR damage corroborated *in vivo* findings (Figure 6 vs Figure 9 – figure

supplement 1). Similarly, we found a general lack of neutrophil response.

Ex vivo: Microglia display dynamic changes in morphology in lesion areas

Without laser damage, microglia exhibited a tiled distribution and stellate

morphology with highly-ramified branching patterns (Figure 9a). 1 day after laser

exposure, microglial somas aggregated to the lesion location. They began to

migrate into the ONL and the most notable phenotype was a change from the

ramified, and pancake-flat morphology seen in the healthy retina, to a dagger-like

axial morphology. (Figure 9a + Video 1). At 3 and 7 days after lesion, microglia

migrated deeper into the outer retina and remained aggregated with an axially

elongated phenotype. 2 months after laser lesion, microglial somas were no

longer found in the ONL. Instead, microglia redistributed similar to that of the

healthy retina (Figure 9a), once again co-stratifying predominantly with the NFL

and plexiform layers of the retina.

Whereas we found a robust response of deep microglia at the OPL to PR

injury, we observed little migratory response of the microglia in the NFL or IPL

(Figure 9 + Figure 9 – figure supplement 1) suggesting axial and lateral

constraints on the extent of microglial recruitment.

Microglia form PR-containing phagosomes

A detailed examination of the microglial involvement with PR somata in response

to PR injury revealed unique microglia-PR interactions within the ONL. In cross-

section, PR cells comprise a large portion of the retina reaching from the outer-

segment tip, inner segments, somata and spherule/pedicle synaptic contacts at

the OPL. Likewise, we saw microglial involvement with all of these layers.

Within 1 day, we found microglial processes interspersed within the dense

aggregation of PR somata within the ONL. Amoeboid cells enveloped the

somata of PR's and phagocytosis was detected 1, 3 and 7 days post-laser

exposure (Figure 9 – figure supplement 2). Confocal microscopy revealed GFP-

positive processes surrounding PR nuclei, engulfing multiple somata (Figure 9 –

figure supplement 2a, c). By 3 days, microglial processes and somas were found

to migrate deeper, now with processes extending into the distal portions of the

PR cells including the inner/outer segments. By two months microglial processes

and somas had retreated out of the ONL.

The DAPI nuclear stain combined with confocal microscopy not only

helped us discern retinal neurons, but also allowed us to differentiate between

microglia and phagocytosed PR's. Two features were different from PR and

microglial nuclei. First, whereas PR's displayed a uniform, homogeneous

nuclear fluorescence, microglial nuclei showed a mottled, and heterogenous

DAPI appearance (Figure 9 - figure supplement 2a). Second, microglia nuclei

were nearly 3x larger in volume compared to healthy and damaged PR nuclei.

Microglia had nuclear volume of 110 ± 42 μm^3 and PR nuclei were 35 ± 5 μm^3 (p

< 0.001, Figure 9 – figure supplement 2b). PR nuclei within microglial

phagosomes displayed similar nuclear volume compared to adjacent PR's in

undamaged locations (Figure 9 – figure supplement 2a).

Ex vivo: **At lesion sites, neutrophils remain within the retinal vasculature**

Corroborating in vivo AOSLO findings we did not find neutrophil aggregation or

extravasation in response to laser damage at any of the time points examined.

Ex vivo microscopy revealed that neutrophils were found within the vascular

network and did not extravasate into the neural retina. Very few neutrophils were

found in lesioned retinas, comparable to the paucity of neutrophils found in

healthy retinas. The few detected neutrophils were remnants of those found

within the capillary network at point of death. Detailed Z-stacks at 60x

magnification revealed "pill-shaped" morphology similar to that seen *in vivo*,

where neutrophils are compressed within capillaries. In one exceptional example

(1 day post-damage, Figure 9c,d), we observed two neutrophils in a single z-

stack, one in a capillary (1) and one at a capillary branch point (2), but none were

observed to have left the confines of the vasculature suggesting they were not

recruited by activated microglia.

Retinal neutrophil concentrations were quantified from larger z-stacks (796

x 796 µm, Figure 10a). Control locations (n = 2 mice, 4 z-stacks) had 15 ± 8

neutrophils per mm^2 of retina whereas lesioned locations (n = 2 mice, 4 z-stacks)

had 23 ± 5 neutrophils per mm^2 of retina (Figure 10b). The difference between

control and lesioned groups were not statistically significant (p = 0.19).

Finally, when we rendered confocal Z-stacks in cross-sectional view, we

discovered that the few fluorescent neutrophils present were found colocalized

within the tri-layered vascular stratifications of the mouse retina [34,55,56]. None

were found in non-vascular layers (Figure 9). Taken together, all *ex vivo* data

indicates that neutrophils remain localized within vessels, suggesting that

neutrophils do not extravasate or aggregate in response to this laser lesion

model, regardless of the robust phagocytic microglial response. These data

corroborate the in vivo findings.

Discussion:

Summary

In many retinal diseases, resident microglial populations are found to exhibit

cross-talk with systemic immune cells[15,18]. The complex temporal dynamics

between resident and systemic immune cells unfolds from seconds-to-months

and has been poorly characterized due to lack of resolution, sufficient contrast

and a non-destructive imaging approach that can track changes over time. Here,

our engineering advance overcomes these limitations by using phase-contrast

and fluorescent imaging with adaptive optics to visualize the interaction of

multiple cell types. With this advanced imaging technology, we reveal the

absence of neutrophil involvement in response to an acute injury, despite

progressive changes in microglial activity and morphology. Here we discuss the

implications of such findings in the context of retinal damage and more broadly,

to retinal disease.

Focal retinal lesions for tracking the immune response

Light damage offers a number of advantages for creating acute damage in the

retina. It offers placement precision that is better controlled than other acute and

invasive methods, such as incision/poke injuries[57], retinal detachment[58] and

chemical injury[59,60]. In the mouse, focal light dosage comes with greater axial

confinement within the retina by nature of the high numerical aperture of the

mouse eye[29] which imposes minimal collateral damage to layers above or below

the plane of focus (Figure 1a). The laser exposure protocol employed here was

highly reproducible as ~95% of light exposures resulted in retinal damage of

similar size and hyperreflective phenotype.

Seminal studies in the brain have used focal light exposure to induce

acute microglial response to targeted areas.[61,62] Since then, it has been a

popular damage model. Focal lesions in the retina have been conducted in a

number of popular animal models including mouse[63,64], macaque[65–67] and

cats.[68,69] Laser damage is also clinically relevant as it is both experienced with

accidental laser exposure[70,71] as well as purposeful ablation used in

photocoagulation and as a therapy for retinal ischemic disease, retinopathy of

prematurity[72] and diabetic retinopathy[73]. Thus our results shed light toward the

immune response that may be imparted due to phototoxic damage. More widely

however, this approach may be considered when investigating how native

microglia may signal to the systemic immune system in response to any acute

injury or chronic photoreceptor loss in aging/diseased retinas.

Titration of the 488 nm laser leads to mild retinal damage

While it is beyond the scope of this report to catalog the vast parameter space in

which light may impose damage in the retina, it is noteworthy to discuss that the

exposure intensity, subtended angle and duration of the CW light source we used

delivered an intentionally mild damage to the retina. Using dosages too high

would run the risk of collateral damage to the blood retinal barrier or Bruch's

membrane[74] which could cause a choroidal neovascularization phenotype[75].

Either of these would be undesirable for studying the native/systemic immune

response as it would potentially confound the traditional extravasation pathways

of the inflammatory system[24,76]. Instead, we chose our laser exposure condition

to impart a weak, but reproducible loss in photoreceptors while minimizing

collateral damage to the cells above and below the plane of focus.

With OCT, we see the primary damage phenotype localized to the

OPL/ONL bands (Figures 1, 2) with visibly undetectable change in the anatomy

of the inner retina. Histology corroborated this finding since the only layer

showing quantifiable cell loss was the photoreceptor layer (Figure 3).

Progressive PR loss and morphology of the lesion tracked over time

The amount of light we delivered did not immediately ablate photoreceptors as

the peak cell loss wasn't observed until 3-7 days after laser exposure suggesting

a progressive damage phenotype of apoptosis or necroptotic death rather than

direct ablation. Histology showed a ~27% reduction in PR nuclei 7 days post

lesion. The total number of PR nuclei within the lesion location returned to values

similar to baseline by 2 months, which was surprising given that PRs do not

regenerate. Our interpretation is that adjacent PRs spill into the region of loss,

similar to what several have described previously[65,77]. Corroborating the

histological finding of mild cell loss, is the in vivo OCT data which shows no

evidence of local edema, cavitation or excavation of the ONL after PR loss

(Figure 2a). The return of the appearance, thickness and redistribution of cells

within the ablated location indicates that retinal remodeling occurs within a 2

month window. The concurrence of microglia in these outer retinal bands (where

they are normally absent in health[78]) support the hypothesis that microglia

localized to this region to facilitate a phagocytic injury response and perhaps

contribute toward synaptic remodeling[11].

The hyperreflective phenotype does not arise from microglia or neutrophils

Light damage is known to create a hyper-reflective bands in OCT imaging [66,79,80].

A common speculation is that the increased backscatter may arise from the local

inflammatory cells that activate or move into the damage location. In our data,

confocal AOSLO and OCT revealed a hyperreflective band at the OPL and ONL

after 488 nm light exposure (Figure 2a, b). However, we found that the

hyperreflective bands appeared within 30 minutes after the laser injury. This

phenotype preceded any detectable microglial migration toward the damage

location (Figure 2 – figure supplement 1 and Figure 6 – figure supplement 1).

We thus conclude that the in vivo hyperreflective phenotype is not caused by

microglial cell activity or aggregation.

Direct activation of microglia from 488 nm light exposure was minimal

It is conceivable that 488 nm light used for either imaging (56 μW) or imparting

damage (785 μW) might activate the GFP-containing microglia in the Cx3CR1

mouse model used here. However, several lines of evidence speak against this

possibility. 1) We did not observe photobleaching of CX3CR1 positive cells in

response to the damage suggesting the fluorescence imaging light was

insufficient to damage microglia. 2) The focal plane was adjusted using the optics

of the AOSLO, focusing the light such that the dose was most axially

concentrated onto the outer retina when performing retinal injury. Thus, the light

dosage received by the microglia above was defocused and less than the

targeted PR layer (Figure 1a). 3) Histology showed no evident necrotic/apoptotic

microglial morphologies and were similar to cells at undamaged locations.

488 nm laser lesion does not photocoagulate or alter retinal circulation

Despite imparting damage to the photoreceptors, the damage regime used here

did not alter the perfusion of the retinal circulation. We show three independent

measures that blood flow is uninterrupted, despite quantifiable PR loss and

activation of microglia. 1) Fluorescein angiography (Figure 1b, bottom) displays

intact vasculature passing through and above lesion locations. The absence of

fluorescein leakage indicates that the lesion did not compromise the blood-retinal

barrier. Additionally, there was no indication of a perforated Bruch's membrane.

2) AOSLO motion contrast vascular maps [25,30,34] displayed persistent blood

perfusion inside vessels near laser lesion sites (Figure 4). This indicated that

single cell perfusion through the capillaries above and adjacent to the regional

damage was maintained 3) Capillary line scans indicate that RBC flux was not

modified at lesion locations and fell within the normal range[30,50] (Figure 4 – figure

supplement 1). Altogether, these three lines of evidence indicate that the 488 nm

light exposure does not impart perfusion changes within the retinal vasculature.

Microglial/neutrophil discrimination using label-free phase contrast

In this work, we use fluorescence to validate the presence and dynamics of

microglia and neutrophils in response to PR damage. We have found that

microglia and neutrophils show a number of differences that may be useful for

identifying their type without the need for fluorescent labels. For example: under

healthy conditions, these cells exhibit morphological differences: retinal microglia

exhibit processes that emanate from the soma, exhibiting an arbor that actively

surveys a large patch of retina, while neutrophils are spheroid, sometimes

presenting as cylinders when squeezing through retinal capillaries. Another

difference lies in their motility: neutrophils remain within the vasculature, often

times traveling at high speeds while microglial somas generally remain stationary

as they monitor the local microenvironment. With a strong base-of-knowledge

about the morphological and behavioral features to expect for each cell type,

label-free imaging could discriminate not just immune cells, but other retinal cells

as well in the future.[24] This is particularly promising when considering translating

these observations into the human population where dyes and fluorescent agents

are used sparingly.

Resident microglia do not need systemic neutrophils for resolution of mild

laser-damage

The CNS and retina, unlike other peripheral tissues, cannot suffer from excess

inflammation as there may be dire functional consequences. Therefore it is

possible that microglia protect against exorbitant inflammation by modulating the

recruitment of systemic inflammatory cells.[4,15–17] Of these, neutrophils are often

one of the first systemic responders. Despite their helpful roles in other tissues,

neutrophils can secrete neurotoxic compounds that could present a danger to the

CNS.[81] Given their conflicted role in the body, we ask the question: to what

extent do neutrophils respond to acute neural loss in the retina? Retinal cells are

lost with age[82] and disease[83] and yet, for the organism, visual perception must

persist. In this laser lesion model, we ablate 27% of the photoreceptors in a 50

µm region. This acute damage model can begin to provide clues about how the

immune system responds when photoreceptors are lost in disease.

We find that microglia undergo a rapid and progressive response to this

injury. We show evidence of PR phagocytosis (Figure 9 - figure supplement 2),

interaction with neighboring microglia (Figure 9 – figure supplement 1) and they

are also axially positioned to facilitate retinal remodeling (Figure 9). Furthermore,

throughout the temporal evolution of the microglial response, we find no evidence

of neutrophil recruitment despite the damage being within 10s of microns from

retinal vessels that carry systemic neutrophils. At the onset of the neutrophil

extravasation cascade, endothelial cells in the vicinity of inflamed tissue typically

elevate the expression of adhesion molecules, facilitating the adherence and

extravasation of circulating neutrophils.[84] Furthermore, neutrophils are

dependent on priming events as prerequisite to further activation and

engagement of their effector functions.[85,86] Based on our data, we suggest that

although microglia show a strong and lasting activation, at no time point from

seconds-to-months, are the damage-associated molecular patterns or

chemotactic gradients strong enough to recruit neutrophils in response to this

damage. This is evidenced in our data from two key observations: 1) in response

to laser injury, we saw no examples of systemic leukocytes rolling in vessels

adjacent to injury locations (Figure 8 – video 1). 2) Using fluorescence, we did

not observe adherent or extravasated neutrophils adjacent to imparted

photoreceptor loss (Figure 8). This may suggest that the region of insult is too

small, or that activated microglia are not sufficient for recruiting neutrophils with

damage of this magnitude. This could mean that a minimum threshold of neural

damage must be met before neutrophils will respond to damage of this type.

Such a strategy would benefit the CNS. It is possible that resident microglia

facilitate the necessary phagocytic and retinal remodeling response despite

release of cytokines from damaged retinal cells that would normally recruit

systemic immune cells in peripheral tissues.

Future work will explore whether there is a threshold magnitude of

neuronal cell loss required for recruitment of systemic cells that is unique to the

retina. Building on this work, next studies will examine more severe or

widespread injury regimes that may provide stronger activating molecular signals

and interact with a larger population of systemic cells.

Microglia may inhibit neutrophil activation

Microglia may be involved in a system that protects the CNS from propagating a

much larger systemic response, potentially exacerbating disease pathologies that

would compromise overall CNS function. From this work, both *in vivo* and *ex vivo*

data corroborate the finding that microglia become reactive, whereas no

evidence of neutrophil recruitment is observed. In another damage model[87], they

report that tissue-resident macrophages may exhibit the capacity to cloak tissue

micro-damage. This offers the possibility that resident immune cells, such as

retinal microglia, can handle small insults without inducing a chemokine cascade

that may invoke a larger systemic response that could further damage the

precious retinal tissue.[88] Regardless of the mechanism, we find that despite a

robust microglial activation that lasts for weeks, at no time point do they recruit

neutrophils. The nuance of this interaction likely represents the fine balance that

facilitates a helpful local response within the CNS that does not impart a more

widespread cytokine storm that may otherwise exacerbate retinal damage.

Further work will explore whether microglia exhibit a cloaking response in the

retina, inhibiting neutrophil or other immune cell extravasation/chemotaxis toward

lesion sites. We expect such work to be pivotal in understanding the balance that

is broken or left unchecked in conditions of autoimmune disease and the

umbrella of diseases that comprise the uveitic response which is a direct threat to

lifelong vision.[89]

Conclusion

Here, we have applied innovative *in vivo* imaging at the microscopic scale to

reveal the cellular immune response to a retina in jeopardy. The dynamic

environment of the retina includes a native population of resident microglia and

systemic immune cells delivered through the vasculature. These two lines of

defense work in concert in the mammalian body and are critical for maintaining

retinal homeostasis. In this work we directly study the interaction between

microglia and neutrophils, two major classes of immune cells that are implicated

in inflammatory initiation, escalation, propagation and debris removal in response

to an acute geographical injury in the retina. Using cutting-edge retinal imaging

modalities, we find that resident microglia become locally activated and regionally

responsive to focal laser lesion. Cells migrate away from their stratified locations

near plexiform layers of the retina and migrate toward the axial site of damage

within hours to weeks after injury. However, systemic neutrophils, which are

typically regarded as first-line responders to tissue damage, are not recruited to

this damage despite neutrophils flowing within 10s of microns away from the

location of damage (Figure 8 – video 2). Beyond the context of this specific

finding, we share this work with the excitement that AOSLO cellular level imaging

may reveal the interaction of multiple immune cell types in the living retina, a

unique tissue in its own regard. By using fluorophores associated with specific

immune cell populations, the complex immune cell dynamics that orchestrate the

immune response may be examined in this specialized tissue and may reveal

further insights to the interactions of single immune cells in the living body in a

non-invasive way.

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Figures & videos:

Figure 1. Laser injury assessed with commercial SLO and OCT. **(A)** 488 nm light
is focused onto the photoreceptor outer segments using AOSLO. Created with
Biorender.com. **(B)** 30° SLO images of NIR reflectance, blue reflectance and
fluorescein angiography of a mouse retina 1 day after laser exposure. Three
focal planes are shown. NIR and blue reflectance reveal small hyperreflective
regions below the superficial plane. Fluorescein reveals intact vasculature with
no sign of leakage. Arrows indicate regions with imparted laser damage (1-4). **(C)**
OCT B-scans passing through laser-exposed regions indicated in B. Exposures
produced a focal hyperreflective band within the ONL with adjacent retina
appearing healthy. OCT images were spatially averaged (~30 μm, 3 B-scans).
Scale bars = 200 μm horizontal, 200 μm vertical.

Figure 2. Laser damage temporally tracked with AOSLO and OCT. Laser-
exposed retina was tracked with OCT **(A)**, confocal **(B)** and phase-contrast **(C)**
AOSLO for baseline, 1, 3, 7 day and 2 month time points. OCT and confocal
AOSLO display a hyperreflective phenotype that was largest/brightest at 1 day
and became nearly invisible by 2 months. Dashed oval indicates region targeted
for laser injury. Phase-contrast AOSLO revealed disrupted photoreceptor soma's
1 day after laser injury. OCT images were spatially averaged (~30 μm, 8 B-
scans). Scale bars = 40 μm, OCT image vertical scale bar = 100 μm.

Figure 2 - figure supplement 1 Lesion location tracked from minutes to 1 day
with OCT. After baseline OCT acquisition, OCT was performed every 5-7
minutes for one hour after 488 nm light exposure. 6 hour and 1 day time points
were subsequently acquired. A band of hyperreflectivity forms near the OPL/ONL
interface within 30 minutes of 488 nm light exposure. Hyperreflective band,
spreads deeper into the ONL within ~1 hour. OCT images were spatially
averaged (~30 μm, 8 B-scans). Scale bar = 40 μm horizontal, 100 μm vertical.

Figure 3. Retinal histology confirms photoreceptor ablation and preservation of inner retinal cells. Cross sectional view **(A)** and en-face **(B+C)** images of DAPI-stained whole-mount retinas (5 mice) at laser injury locations over time. By 1 day, ONL becomes thicker at lesion location, but thinner by 3 and 7 days. By 2 months, the ONL appeared similar to that of control. The inner (**B**, solid rectangle) and outer (**C**, dashed rectangle) stratum of ONL show axial differences in ONL loss**.** Most cell loss was seen in the outer aspect of the ONL **(C)**. Scale bars = 40 μm. **(D)** Cross section of DAPI-stained retina displaying INL and ONL regions for quantification. Each analysis region was 50 μm across and encompassed the entire INL or ONL. **(E)** En-face images show 50 μm diameter circles used for analysis. **(F)** Nuclei density for control and post-injury time points. ONL nuclei were reduced at 3 and 7 days (p = 0.17 and 0.07 respectively) while INL density remained stable (n = 10 mice, 3 unique regions per time point). Error bars display mean ± 1 SD.

Figure 4. Microvascular perfusion unchanged after laser damage. A single
location tracked over time and at three vascular plexuses using AOSLO. Motion-
contrast images were generated from confocal videos to reveal vascular
perfusion status. Retinal vasculature remained perfused for all time points
tracked and at all depths. White oval indicates damage location. Scale bar = 40
µm.

Figure 4 – figure supplement 1 Measurement of single-cell blood flux after
laser damage using phase contrast AOSLO. **Mouse 1: (A)** The vascular plexus
corresponding to IPL (cyan) and OPL (red) were targeted for flux determination. Blood
cell flux was measured for 2 capillaries within the same field, at different depths. Arrows
show the location for repeated line scan acquisitions. **(B)** RBC flux images were tracked
up to 7 days post-damage. Scale bars = 10 ms, horizontal and 5 μm vertical. **(C)**
Capillary flux measurements over 7 days. Despite the outer capillary displaying higher
flux, both inner and outer capillaries changed synchronously for each time point. **(D)**
Correlation of inner and outer capillary flux. Linear regression model displays a weak
positive correlation (black dotted line). **Mouse 2: (E)** Left: Representative 55° SLO
image showing regions targeted for capillary flux measurement. One region was subject
to 488 nm laser damage and the other was left unlasered (Control). Scale bar = 200 μm.
Right: Capillaries targeted for blood cell flux measurement. Arrows show the location for
repeated line scan acquisitions. Scale bar = 40 μm. **(F)** RBC flux images were tracked
up to 2 months post-damage. Scale bars = 10 ms horizontal and 5 μm vertical. **(G)**
Capillary flux remained similar at lesion and control locations over all time points
assessed. Gray shaded regions indicate range for normal capillary flux in the healthy
C57BL/6J mouse (Dholakia et al 2022). **(H)** Correlation of flux in lesion and control
locations. Linear regression model displays a positive correlation (black dotted line).

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Figure 5. Microglial response 1 day after laser injury imaged in vivo with
fluorescence SLO and AOSLO. **(A)** Left: Deep-focus NIR SLO fundus image (55°
FOV) of laser-injured retina. White arrowheads point to damaged locations
showing hyperreflective regions. Inset scale bar = 40 µm. Right: Fluorescence
fundus image from same location. Fluorescent CX3CR1-GFP microglia are
distributed across the retina and show congregations at laser-damaged locations.
Scale bar = 200 µm. **(B)** Magnified SLO images of microglia at laser-damaged
and control locations (indicated in A, right, white boxes). Control location displays
distributed microglial whereas microglia at the lesion location are bright and
focally aggregated. **(C)** Fluorescence AOSLO images show greater detail of cell
morphology at the same scale. In control locations microglia showed ramified
morphology and distributed concentration whereas damage locations revealed
dense aggregation of many microglia that display less ramification. Scale bars =
40 µm.

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1021   **Figure 5 – video 1** Dynamic pseudopodia imaged with phase-contrast AOSLO 1
1022   day post-injury. At the OPL/ONL border, a putative microglial pseudopod
1023   extension was captured among a field of static, disrupted PR somas. Video is 3
1024   minutes elapsed. Scale bars = 20 μm.

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Figure 6. Microglial response to laser injury tracked with AOSLO. Simultaneously acquired NIR confocal and fluorescence AOSLO images across different retinal depths. Data are from one CX3CR1-GFP mouse tracked for 2 months. Microglia swarm to hyperreflective locations within 1 day. Microglia maintain an aggregated density for days and resolve by 2 months after damage. Scale bar = 40 μm.

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Figure 6 – figure supplement 1 Hyperreflective appearance emerges before microglia swarm to damage location. AOSLO confocal and fluorescence images were acquired for baseline, 30, 90 minute and 1 day post-laser exposure. The hyperreflective phenotype appeared within 30 minutes post damage. Microglia were not found to aggregate until ~1 day after. Scalebar = 40 μm.

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Figure 7. Neutrophil morphology imaged in vivo using AOSLO. **(A)** Phase-
contrast, motion-contrast and fluorescence AOSLO reveal the impact of passing
neutrophils on single capillaries. A rare and exemplary event shows a neutrophil
transiently impeding capillary blood flow for minutes in healthy retina. Scale bar =
40 μm. **(B)** In-vivo AOSLO and ex-vivo fluorescence microscopy show
neutrophils in two states. Neutrophils within capillaries displayed elongated,
tubular morphology. Extravasated neutrophils were more spherical. Bottom
images show extravasated neutrophils in response to LPS model for comparison
(not laser damage model). Scale bar = 20 μm.

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Figure 7 – video 1 Neutrophil dynamics within a primary retinal vessel in a
Catchup mouse. Confocal (left) and fluorescence (right) AOSLO were acquired
from a large primary retinal vessel simultaneously. Several quickly flowing
neutrophils are seen as streaks within the lumen of the large retinal vessel. Video
plays in real-time (25 FPS, 20 seconds). Scale bar = 20 μm.

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Figure 7 – video 2 Neutrophils imaged in capillaries of a Catchup mouse.
Motion-contrast (left) and fluorescence (right) AOSLO show a single neutrophil
moving through a branch of the OPL capillary network. Red circles/arrows
indicate neutrophil path within the vascular perfusion map. Rare neutrophils were
found to move slowly through capillaries. Video is 0.4 seconds elapsed. Scale
bar = 20 μm.

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Figure 8. Retinal damage location tracked with AOSLO does not show accumulation of neutrophils. A single retinal location was tracked in a Catchup mouse from baseline to 2 months after lesion. Location of the lesion is apparent at 1 and 3 days post injury with diminishing visibility after 1 week. Despite the ability to detect neutrophils (Figure 7), we did not observe stalled, aggregated or an accumulation of neutrophils at any time point evaluated. This evaluation was confirmed at multiple depths ranging from the NFL to the ONL of the retina in vivo. Scale bar = 40 μm.

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Figure 8 – video 1 Neutrophil dynamics within a primary retinal vessel in a
Catchup mouse 1 day after a deep retinal laser lesion is placed nearby. Confocal
(left) and fluorescence (right) AOSLO images were acquired simultaneously.
Quickly flowing neutrophils are seen as streaks within the lumen of this large
retinal vessel and despite the adjacent deep retinal lesion (within 100 μm), there
is no indication of rolling or crawling neutrophils. Video plays in real-time (25
FPS, 20 seconds). Scale bar = 20 μm.

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Figure 8 – video 2 Neutrophil dynamics within an OPL capillary in a Catchup
mouse 1 day after deep laser injury. Motion-contrast (left) and fluorescence
(right) AOSLO are displayed in tandem. At 1 day post-laser injury, a single
neutrophil is seen moving through a capillary that runs directly through the injury
site (yellow oval). Despite injury, neutrophil does not slow or stall at the lesion
location. Video is 0.68 seconds elapsed. Scale bar = 20 μm.

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Figure 9. Neutrophil behavior under laser injury, as observed through ex vivo
confocal microscopy, remains unresponsive despite marked microglial activation
(A) En-face max intensity projection images of inner and outer (separated by
approximate INL center) retinal microglia/neutrophils in Ly-6G-647-stained
CX3CR1-GFP retinas. Microglia display focal aggregation in the outer retina for
1, 3 and 7 day time points that is resolved by 2 months. Neutrophils do not
aggregate or colocalize to the injury location at any time point. Z-stacks were
collected from 5 mice for the indicated time points. **(B)** Cross-sectional views of
en-face z-stacks presented in A, including DAPI nuclear label. White dotted line
indicates 100 µm region expanded below. Microglia migrate into the ONL by 1, 3
and 7 days post-laser injury and return to an axial distribution similar to that of
control by 2 months. The few neutrophils detected remained within the inner
retina. Scale bars = 40 µm. **(C)** Orthogonal view of DAPI-stained retina with Ly-
6G-647-labelled overlay 1 day post-laser-injury. In a rare example, 2 neutrophils
are found within the IPL/OPL layers despite a nearby outer retinal laser lesion.
Scale bar = 20 µm. **(D)** Magnified 3D cubes representing cell 1 and 2 in C. Cell 1
displays pill-shaped morphology and cell 2 is localized to a putative capillary
branch-point. Each are confined within vessels suggesting they do not
extravasate in response to laser injury.

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Figure 9 – figure supplement 1 Neutrophil/microglial response to laser injury
tracked with *ex vivo* confocal microscopy. Simultaneously acquired GFP-positive
microglia and Ly-6G-647-positive neutrophils were imaged with confocal
microscopy in 5 CX3CR1-GFP mice. En-face images for several retinal depths
are displayed. By 1, 3 and 7 days post-lesion, microglia have migrated into the
outer retina, many appearing amoeboid and displaying fewer laterally-branching
projections. Despite the deep microglial response, neutrophils stay within the
inner retina and are not found in the avascular outer retinal layers. Scale bar = 40
μm.

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Figure 9 – figure supplement 2 Microglial PR phagosomes in the outer retina
assessed with *ex vivo* confocal imaging. **(A)** En-face images of outer ONL in a
DAPI-stained CX3CR1-GFP mouse 3 days post-laser-injury (top row). Microglia
have infiltrated deep into the ONL and several PR phagosomes were identified.
White arrows indicate locations for a single microglia (i), PR (ii) and PR
phagosome (iii). These locations were expanded and displayed below. Microglia
exhibited a heterogeneous nuclear staining pattern while PR nuclei exhibited
homogenous DAPI fluorescence pattern. PR's displayed this pattern regardless
of whether they were within a microglial phagosome or not. Top scale bar = 20
μm, bottom scale bar = 2 μm**. (B)** A finely-sliced (0.1 μm step size) outer retinal z-
stack of DAPI-stained CX3CR1-GFP retina was used to quantify the average
nuclear volume for infiltrated microglia (n = 14 nuclei) and PR's (n = 20 nuclei) for
the same lesion site presented in A. On average, microglia had a statistically
significant (p < 0.001) nuclear volume that was >3x that of PR's. These
measurements allowed us to discriminate microglial somas from PR
phagosomes. Error bars display mean + 1 SD. **(C)** Cross sections of DAPI-

stained outer retina in CX3CR1-GFP mice for 1, 3 and 7 days post-laser injury (n=3 mice). 3 representative planes (X-Z) through the lesion are displayed for each time point. Microglia form PR phagosomes within the ONL and microglial processes were seen extended into the PR inner/outer segment layer. Arrows label various morphological features seen at lesion sites: microglial somas (yellow), diving microglial process (violet), PR phagosome (red), microglial inner/outer segment process (cyan). Scale bar = 20 μm.

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Figure 10. Quantification of neutrophils in laser damaged retinas assessed with
ex vivo confocal microscopy over a wide-field. **(A)** Representative image displays
neutrophils quantified using large-field (796 x 796 µm) z-stacks for control or 1
day after injury time points. In both control and laser injured retinas, neutrophils
were sparse and confined to locations within capillaries suggesting they were the
native fraction of circulating neutrophils at time of death. Inset displays expanded
image of a single neutrophil. Scale bar = 200 µm. **(B)** Neutrophils quantified and
displayed as the number of neutrophils per retinal area. The difference in number
of neutrophils in control vs lesioned retinas was not statistically significant (p =
0.19). Error bars display mean + 1 SD.

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Video 1 Rotating 3D cubes of outer retinal nuclei and microglia after focal laser
injury. Outer retinal Z-stacks of DAPI-stained whole-mount CX3CR1-GFP retinal
tissue were imaged for control, 1, 3, 7 day and 2 month time points (n = 5 mice).
DAPI + microglia composite cubes are displayed above and microglia cubes are
displayed below. By 1 day, microglia send projections into the ONL, by 3 and 7
days, microglial somas have migrated into the ONL. Microglia within the ONL
exhibit different morphology compared to the baseline condition. By 2 months,
microglia are found back within the OPL, exhibiting lateral projections, similar to
baseline. Scale bar = 40 μm.

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Video 2 Rotating 3D cubes of single neutrophils after laser injury or endotoxin
induced uveitis. *Ex vivo* confocal z-stacks (0.1 μm steps) allowed detailed
visualization of single neutrophils at 1 day after laser injury or 1 day after
intravitreal LPS injection. After laser injury, neutrophils maintain a tubular, pill-
shaped morphology (left). Occasionally, they would come to rest at capillary
branch points (middle). In the EIU model, neutrophils extravasate into the retinal
parenchyma and exhibit more spheroid morphology (right). We did not observe
neutrophils to exhibit the extravasated morphology in response to laser injury.

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	Superficial	Deeper	Deepest
NIR reflectance	1, 3, 2, 4		
blue reflectance			
Fluorescein			

	Baseline	1 day	3 day	7 day	2 month
OCT (A)					
AOSLO Confocal (B) OPL/ONL					
Phase Contrast (C) ONL			Not acquired		

	Baseline	**1 day**	**3 day**	**7 day**	**2 Month**
NFL	NIR Confocal / Neutrophil				
IPL					
INL					
OPL					
ONL					
ONL/IS					

A Neutrophils – large-field projection

Neutrophils counted

B P = 0.19

Mouse 1 – Flux measured for axially separate capillaries

A

IPL

OPL

AOSLO motion contrast

Inner capillary

Outer capillary

B

Outer   Inner

Baseline
1 day
3 day
7 day

C

RBC Flux (cells/s)

Outer   Inner

Baseline, 6 min, 17 min, 27 min, 39 min, 50 min, 62 min, 69 min, 1 day, 3 day, 7 day

D

Outer Cap. flux

$y = 0.3389x - 6.1277$
$R^2 = 0.59$

Inner Cap. flux

Mouse 2 – Flux measured for laterally separate capillaries

E

Control   Lesion

AOSLO motion contrast

OPL

OPL

F

Lesion   Control

Baseline
6 hour
1 day
3 day
7 day
2 month

G

RBC Flux (cells/s)

Lesion   Control

Baseline, 10 min, 20 min, 30 min, 40 min, 50 min, 6hr, 1 day, 3 day, 7 day, 2 month

H

Lesion Cap. Flux

$y = 0.7441x + 51.902$
$R^2 = 0.7786$

Control Cap. Flux

A

	Microglia	DAPI	Merged
ONL - Outer	iii, ii, i		
Microglia i		V = 124 µm³	
PR ii		V = 38 µm³	
PR phagosome iii		V = 34 µm³	

B

P < 0.001

Nuclear Volume (µm³)

PR's   Microglia

C

	Slice 1	Slice 2	Slice 3
1 day	DAPI / Microglia		
3 day			
7 day			

Microglial soma/diving microglial process/PR soma
phagosome/Microglia inner segment process