Dynamics of pitch perception in the auditory cortex

*Ellie Bean Abrams[1,2,3], Alec Marantz[1,4], Isaac Krementsov[5], and Laura Gwilliams[6]

1: New York University; Department of Psychology

2: Center for Language, Music, and Emotion (CLaME), New York University

3: Music and Audio Research Laboratory (MARL), New York University

4: New York University; Department of Linguistics

5: Stanford University; Department of Statistics

6: Stanford University; Department of Psychology

* Corresponding author: ellie.abrams@nyu.edu

Abstract

The ability to perceive pitch allows human listeners to experience music, recognize the identity
and emotion conveyed by conversational partners, and make sense of their auditory
environment. A pitch percept is formed by weighting different acoustic cues (e.g., signal
fundamental frequency and inter-harmonic spacing) and contextual cues (expectation). How
and when such cues are neurally encoded and integrated remains debated. In this study,
twenty-eight participants (16 female) listened to tone sequences with different acoustic cues
(pure tones, complex missing fundamental tones, and tones with an ambiguous mixture), placed
in predictable and less predictable sequences, while magnetoencephalography was recorded.
Decoding analyses revealed that pitch was encoded in neural responses to all three tone types,
in the low-to-mid auditory cortex and sensorimotor cortex bilaterally, with right-hemisphere
dominance. The pattern of activity generalized across cue-types, offset in time: pitch was
neurally encoded earlier for harmonic tones (~85ms) than pure tones (~95ms). For ambiguous
tones, pitch emerged significantly earlier in predictable contexts than unpredictable. The results
suggest that a unified neural representation of pitch emerges by integrating independent pitch
cues, and that context alters the dynamics of pitch generation when acoustic cues are
ambiguous.

Keywords: *pitch, MEG, auditory, music, acoustic, context*

Significance Statement

Pitch enables humans to enjoy music, understand the emotional intent of a conversational partner,
distinguish lexical items in tonal languages, and make sense of the acoustic environment. The study
of pitch has lasted over a century, with conflicting accounts of how and when the brain integrates
spectrotemporal information to map different sound sources onto a single and stable pitch percept.
Our results answer crucial questions about the emergence of perceptual pitch in the brain: namely,
that place and temporal cues to pitch seem to be accounted for by early auditory cortex, that a
common representation of perceptual pitch emerges early in the right hemisphere, and that the
temporal dynamics of pitch representations are modulated by expectation.

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Conflict of interest
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INTRODUCTION

Pitch is central in appreciating musical melody, understanding the emotional state and intonational intent of a speaker, distinguishing lexical items in tonal languages, and correctly parsing the acoustic environment (de Cheveigné, 2010). This is enabled by the auditory system's ability to map different sound types (e.g., a note played on a piano or a cello or sung by a human voice) onto a putatively unique and stable pitch percept.

The perception of pitch arises from a number of sources in the acoustic input. Fundamental frequency (F0), the lowest periodic component present in the acoustic signal, exhibits a strong influence on pitch perception: a pure sinusoidal tone that repeats 440 times per second will be perceived with 440 Hz pitch (de Cheveigné, 2005). Sounds arising from musical instruments or voices comprise F0 as well as a rich harmonic structure at integer multiples of F0. The spacing between harmonic components likewise exhibits a strong influence on pitch perception. Even if the energy at F0 is removed entirely, listeners perceive the signal as eliciting the same pitch percept (Seebeck, 1841; Schouten, 1938; Licklider, 1954). This "missing fundamental" phenomenon is an important clue to how the auditory system extracts pitch from auditory inputs (Plack et al., 2005; Griffiths and Hall, 2012; Wang and Walker, 2012).

How different spectrotemporal cues are integrated to solve the mapping from acoustic waveform to pitch percept, remains unknown (de Cheveigné, 2005; Oxenham, 2012). Auditory pitch determination begins at the cochlea, where frequencies are mapped to locations along the basilar membrane (Shera et al., 2002, 2010). This organization is preserved as auditory information is transmitted along the afferent auditory pathway (Oxenham and Wojtczak, 2010). The precise ways in which frequency and harmonic information are differentially represented once they reach the primary auditory cortex have been a point of contention, with tonotopy in some cases appearing to represent perceptual pitch (Pantev et al., 1989; Pantev et al., 1996; Monahan et al., 2008) and in other cases showing that the frequency of pure tones is organized tonotopically, with a separate representation of timbre (Langner et al., 1998; Warren et al., 2003; Bizley et al., 2009; Allen et al., 2017). Studies mapping pitch have typically used perceptually unambiguous, narrowband signals as pitch-evoking stimuli (pure tones, ripple-induced noise, relative intensity noise), making it unclear whether these representations track perceptual pitch invariant to spectral structure (Allen et al., 2022) or whether they reflect an F0 extraction mechanism (Kumar et al., 2011b; Griffiths and Hall, 2012). To further complicate this issue, populations of neurons in immediate proximity to spectrally invariant pitch-selective neurons have been shown not to respond to pure tones, but to respond to complex tones and other narrow- or wideband stimuli (Bendor and Wang, 2005). Regarding spectral structure, some auditory neurons are sensitive to spectral contrast, or the difference in intensity between frequency components in wideband stimuli, highlighting spectral shape as a crucial dimension across which stimuli may be represented (Barbour and Wang, 2003). Lastly, listening context (i.e., interspersing stimuli with silence vs. noise) may modulate pitch sensitivity for some auditory regions, but not others (Garcia et al., 2010).

Pitch-selective cortical regions, or, "pitch centers," have been established in lateral Heschl's
gyrus, planum temporale, and superior temporal gyrus (Patterson et al., 2002; Hall and Plack,
2009; Gander et al., 2019; Kim et al., 2022), as well as in anterior non-primary areas (Penagos
et al., 2004). This diversity of cortical representation could be driven by stimulus properties, with
some areas demonstrating a preference for resolved harmonics (Norman-Haignere et al., 2013)
or reflecting one specific stimulus feature (Barker et al., 2011). Alternatively, these areas could
comprise a distributed system of neural ensembles representing pitch over auditory cortex
(Griffiths et al., 2010; Kumar et al., 2011a; Allen et al., 2022). The use of more temporally
resolved methods (EEG/MEG/local field potentials) has allowed for an exploration of pitch
perception at the millisecond level, but work has focused on singular evoked responses as
opposed to the unfolding of a percept over time (Brattico et al., 2001; Loui et al., 2009; Butler
and Trainor, 2012; Kim et al., 2022).

An additional cue to pitch perception is the context in which a sound occurs (Krumhansl and
Shepard, 1979; Krumhansl and Cuddy, 2010; Slana et al., 2016), which has been shown to bias
perception towards a contextually appropriate interpretation when two acoustic cues are
ambiguous or in conflict (Shepard, 1964; Deutsch, 1992; Deutsch et al., 2008). Further, when
there is a high tonal expectation of the next pitch, the expected pitch is neurally represented
even when omitted from the end of a sequence (Berlot et al., 2018). This effect is demonstrably
present as early as primary auditory cortex (Englitz et al., 2024), suggesting that context is a
fundamental component of cortical pitch encoding. However, it is unknown how contextual
expectation interacts with acoustic content to derive an ultimate pitch representation.

In the current study, we aim to disentangle these three primary cues to pitch perception: F0,
inter-harmonic spacing, and tonal context. Magnetoencephalography (MEG) data were collected
from 28 healthy adults presented with sequences of pitch-matched tones with varying spectral
content in and out of context. Pure tones and missing fundamental (MF) complex tones were
used to represent F0 pitch cues and inter-harmonic spacing pitch cues, respectively. Ambiguous
tones were used to investigate the neural representation of pitch in acoustic ambiguity.
Decoding analyses were applied to the MEG data to test hypotheses about shared
representations between tone types. The results provide new evidence for the cortical timing
associated with the analysis of these basic cues to pitch.

MATERIALS AND METHODS

Participants

We recruited 28 participants from the NYU Abu Dhabi community (16 females, mean age 24.8
years). All subjects reported normal hearing and no history of neurological disorders.
Participants were compensated for their time at a rate of 60 dirhams per hour. The experiment
was approved by the NYU Abu Dhabi IRB committee.

Stimuli

Pure tones consisted of one frequency band at F0 with no additional harmonic components, for
a total of 17 unique frequencies (Figure 1A, D). Complex missing fundamental (MF) tones
consisted of the five integer multiples (partials) above, but not including the fundamental
frequency for each of the 18 pitches (Figure 1A, D). For example, a complex MF tone with
energy at frequencies 440, 660, 880, 1100 and 1320Hz has a distance of 220Hz between each
harmonic and will be perceived as having a pitch of 220Hz; yet the 220Hz frequency content
itself is not present. These missing fundamental tones had a flat spectral envelope, with equal
attenuation of all five harmonics.

To build ambiguous tones, we use Diana Deutsch's adaptation of the Shepard tone illusion, in
which she systematically varied the amplitudes of odd and even harmonics across the
semitones spanning one musical octave, resulting in a set of 7 tones corresponding to the notes
of a diatonic scale. Due to the ambiguity of the tones, when they are played in succession
repeatedly, the sequence of tones evokes an auditory barbershop effect, sounding like a
continuously ascending or descending scale with no stable perceived switch during the point at
which the tones repeat. Because of competing pitch cues, namely the actual fundamental
frequency in tension with the spacing between harmonics, the tonal center (i.e., the key of the
scale) may be perceived as either the low or high octave of the scale. Concretely, as the tones
decrease in fundamental frequency, the even harmonics remain the same in amplitude, while
odd harmonics decrease. This leads to competing cues to pitch, namely, a ratio of 2*F0
between harmonics and a highly attenuated, albeit present, F0. Though participants were only
presented with the 7 semitones making up the major scale, 12 complex MF tones were created
to maintain equal stepwise attenuation of the odd harmonics. Each contained the first six
partials (multiples of F0). The parameters used to achieve ambiguity, starting at the top of the
scale, were: Partials 2 and 4 remained flat for all tones, while partials 1 and 3 were attenuated
by 3.5 dB with each semitone decrease in f0. Partial 5 was attenuated to 28 dB for all
semitones. Lastly, partial 6 began at 28 dB and was strengthened by 3.5 dB with each semitone
decrease in F0 (Figure 4D).

Pure, missing fundamental and ambiguous tones were synthesized in three musical keys: A3
(220-440Hz), C4 (262-524Hz), and Eb4 major (312-624Hz; Figure 1C). Frequency values were
calculated according to the equal tempered scale, in which semitones are separated by
constant frequency multiples. These frequencies ranged from 220-624 Hz. These three banks of
tones, corresponding to the three experimental blocks (pure, complex MF, and ambiguous),
were created using PyAudio, a python package for playing and recording audio on Mac OS X.
Tones were saved as wav files with a sampling rate of 44,100 Hz. All tones were 300ms in
duration, 32 bits per sample, and normalized to 70 dB using Praat.

EXPERIMENTAL DESIGN AND STATISTICAL ANALYSES

All tones were presented for a duration of 300ms, with a 200ms silent inter-stimulus interval.
Pure and complex MF blocks each contained nine mini-blocks: up, down, and random for each
of the three musical scales. Each mini-block repeated the 8 tones 15 times, with tone order
depending on the condition. In the up and down conditions, the tones were presented in

ascending and descending order, respectively, with a jittered 500-750ms of silence in between
each mini-block. In the random condition, the 8 tones were presented in random order 15 times.
All mini-blocks were shuffled within larger pure tone and complex MF tone blocks.
177
Participants were presented with the ambiguous tones in a scale condition which mirrored that
of the pure and complex MF tones. Because there are only 7 ambiguous tones per scale, we
played the ambiguous tone at both the beginning and end of the scale so that it would explicitly
act as the low and high octave (Figure 1D). The scale condition was presented in ascending (up
condition; Figure 1C) and descending (down condition) order. As in the pure and complex MF
scale conditions, repetitions were separated by a pause of 500-750ms. Lastly, during the
random condition, the 7 tones were presented in random order 15 times. These 15 mini-blocks
were shuffled.
186
187 All tones were presented binaurally to participants through earphones in the magnetically
188 shielded room (MSR). Participants listened passively, while watching silent videos of nature
189 scenes. Eye tracking was used to ensure participants were not falling asleep. Block order was
190 counterbalanced across participants. The experiment lasted around 80 minutes.
191
192 *Data acquisition and preprocessing*
193
Prior to recording, each subject's head shape was digitized using a Polhemus dual source
handheld FastSCAN laser scanner. Digital fiducial points were recorded at five points on the
individual's head: the nasion, anterior of the left and right auditory canal, and three points on the
forehead. Marker coils were placed at these same points to localize each subject's skull relative
to the MEG sensors. To correct for movement during recording, measurements from the marker
coils were obtained immediately before and after the protocol.
200
Continuous MEG data were recorded using a 208-channel axial gradiometer system (Kanazawa
Institute of Technology, Kanazawa, Japan) with an online bandpass filter of 0.1-200Hz at a
sampling rate of 1000Hz. Continuous recording was noise reduced using Continuously Adjusted
Least Squares Method (CALM) (Adachi et al., 2001), with MEG160 software (Yokohawa Electric
Corporation and Eagle Technology Corporation, Tokyo, Japan). The noise-reduced MEG
recording, digitized head-shape, and sensor locations were then imported into the Python
package *mne* (Gramfort et al., 2013). After visual inspection, one saturated channel was
rejected in two subjects. No channels were rejected in the remaining subjects after visual
inspection. An independent component analysis was fitted on the data to account for 90% of
explained variance, and components corresponding to EKG, eye movements, and blinks were
removed.
212
213 Epochs were extracted from -200ms pre-stimulus onset to 600ms post-stimulus onset, and
214 down-sampled to 200 Hz. Individual epochs were rejected using an absolute threshold of ±2000
215 femto-tesla; less than 5% of epochs were rejected in all subjects. See Figure 1B for evoked
216 responses averaged across subjects, for each experimental condition.
217

218 *Source Localization*
219
220 To perform source localization, the location of the subject's head was co-registered with respect
221 to the sensory array in the MEG helmet. Structural Magnetic Resonance volumes (T1s) were
222 collected from all participants using NYUAD's MRI facility (3T MAGNETOM Prisma, Siemens).
223 These anatomical scans were rotated and translated using *mne* to minimize the distance
224 between the fiducial points of the MRI and the head scan.
225
Next, a source space was created, consisting of 2562 potential electrical sources per
hemisphere using an "ico-4" source space. At each source, activity was computed for the
forward solution with the Boundary Element Model (BEM) method, which provides an estimate
of each MEG sensor's magnetic field in response to a current dipole at that source. The inverse
solution was computed from the forward solution and the grand average activity across all trials.
Data were converted into noise-normalized Dynamic Statistical Parameter Map (dSPM) units
(Dale et al., 2000), using an SNR value of 2. The inverse solution was applied to each trial at
every source, for each millisecond defined in the epoch, employing a fixed orientation of the
dipole current that estimates the source normal to the cortical surface and retains dipole
orientation.
236
237 *Multivariate decoding analysis*
238
239 We implemented our decoding analysis using the Python packages *mne* (Gramfort et al., 2013)
240 and *scikit-learn* (Pedregosa et al., 2011).
241
242 We regularize model fit using L2 regularization, with a fixed strength of alpha=1e+8.
243
244 Before fitting the decoder, we normalize the magnitude of the MEG sensors using
245 *StandardScaler*, a function of *scikit-learn*:
246
247 $z = (x – u)s$
248
where u is the mean of the training samples and s is the standard deviation of the training
samples.
For cross validation, we first randomly shuffle the order of trials. Then we subset the data into
five partitions of 80% - 20% splits, with non-overlapping trials across split assignment. This was
implemented using the KFold (k=5) cross validation scheme in *scikit-learn*. The 80% of trials we
used to train the decoder (i.e., learn the coefficient weights that optimally map the MEG sensor
activity to the stimulus feature), and the remaining 20% of the trials to generate stimulus
predictions based on the learned coefficient maps. We repeat this fit-predict procedure for each
of the 5 folds of the data and average the decoding performance across the five folds.
258
Decoding analyses were applied to the 200 Hz bandpass-filtered epochs. The shape of the
neural data matrix per subject was number of trials (7650) x number of MEG sensors (208) x

number of timesamples from -200:600ms at 200 Hz (161) x number of subjects (28). This neural
data matrix was used for all decoding analyses.

We also derive a corresponding stimulus feature vector, which contains the same number as
trials as the neural data. For example, the stimulus vector that defines musical pitch includes all
the pitch values of each trial (e.g., 440Hz, 312 Hz, etc.); the stimulus vector that defines
categorical tone type includes the tone type of each trial, such as "pure tone", "complex MF
tone", etc.

To address the question of whether a stimulus feature of interest is present in neural responses,
we derived a *decoding accuracy timecourse*. For categorical stimulus features, such as tone-
type, we use a Logistic Regression classifier. In this case, we transform the category labels into
binary [0, 1] sequences, and use one-versus-all Logistic Regression. The performance of this
classifier is quantified using receiving operator characteristic area under the curve (ROC AUC),
by comparing the true binary property of the feature [0, 1] to the probabilistic output of the
classifier, bounded between 0-1. Chance-level performance of AUC correlation is 0.5.

For continuous stimulus features, such as pitch, we used Ridge Regression. We scaled the
stimulus values linearly between 0-1, such that the lowest value is assigned 0, the highest value
is assigned 1, and the relative distance between values is preserved in the scaled space. We
computed performance using a Spearman rank correlation, which compares the continuous true
property of the feature to the continuous predicted property of the feature. Chance-level
performance of a Spearman correlation is 0. Because a rank correlation metric was used, the
distances between frequencies did not matter. Thus, using log scale as opposed to linear would
not affect decoding performance.

Decoding models were fit for each subject independently, and a separate model was fit at each
time-lag relative to tone onset. That means that we fit a total of 161 x 28 = 4,508 models. The
input to each model is the strength of neural activity in units of femto-tesla across all MEG
sensors across trials.

The step-by-step procedure to derive a decoding timecourse for each subject is as follows: we
loop through each timepoint (161) and K fold (5 subsets of training and testing epochs) and fit a
decoder on the MEG activity (7650 trials total; X) and corresponding stimulus features (tone-
type or pitch; y) at each *training epoch* at that timepoint. We use this classifier to predict
stimulus features for unseen *testing epochs* at that same timepoint. Lastly, we compute
performance by comparing the prediction output by the decoder with the true feature of the
testing epochs.

To address the question of how information is spatially encoded in the brain, we can similarly
derive a *spatial* map of decoding performance by using the same analysis logic, but transposing
space and time. In other words, whereas to derive a decoding timecourse we fit a decoding
model at each time-step separately and used the activity over sensors as the neural features,
we can instead model each reconstructed neural sources separately and use the strength of

activity across time-steps as the neural features. We decided to focus this analysis on the
100ms around the peak of acoustic decoding (see Source Localization, above).
307
308   The step-by-step procedure for spatial decoding is like that of sensor space decoding, but
309   instead of looping through timepoints we loop through each spatial source and fit the decoder
310   on activity during 50ms windows throughout the entirety of the epoch (-200 - -150ms through
311   550-600ms).
312
313   *Second-order statistical tests*
314
To assess statistical significance of decoding analyses in sensor space, we compared the
distribution of decoding performance across subjects against chance performance. Concretely,
we formulated a matrix of shape nsubjects (28) x ntimes (161) and fit a one-sample permutation
cluster test to derive putative clusters of significance (implemented in
mne.stats.permutation_cluster_1samp_test in *mne-python).* This test first performs a t-test for
the distribution of decoding performance across subjects compared to chance level (0.5 for AUC
and 0 for Spearman). This array of t-values is then clustered based on adjacent values (either in
time, or in space, depending on the analysis), that exceed a significance threshold of $t > 1.96$
(equivalent to $p < .05$). Then, the average t-value in the cluster is recorded. Finally, surrogate
data are formed by randomly flipping the sign of the input data. So, the score will be randomly
assigned a positive or negative value, arbitrarily above or below chance. Then, the t-tests and
clusters are re-formed based on this chance-derived surrogate data. This surrogate procedure
is repeated 1000 times to form a distribution of average t-values for clusters. We then count the
number of times that a surrogate t-value magnitude was equal to or greater than the critical
observed t-value in the data. This count divided by the 1000 surrogate values forms our
statistical p-value. For example, to derive a p-value of $p < .05$, there would be no more than 50
surrogate t-values that exceeded the empirical data.
332
To evaluate statistical significance of source decoding within an ROI, we extract the R/AUC
values within each ROI for each subject, for each hemisphere. The statistical significance of
decoding in a given ROI is calculated by averaging the R/AUC values across sources in the
ROI, and then performing a one-sample t-test of the Spearman R or AUC values of these
sources against chance (0 or 0.5, respectively), and a paired t-test comparing scores between
hemispheres.
339
340   **RESULTS**
341
Our use of stimuli with non-overlapping spectral content allowed us to take advantage of the
ability for F0 (*pure tones),* on the one hand, and inter-harmonic spacing F0 (*complex missing
fundamental (MF) tones*), on the other, to convey pitch-relevant information *independently*. Our
use of stimuli with an ambiguous mixture of acoustic cues (*ambiguous tones*), which elicit
distinct pitch percepts depending on context (Deutsch et al., 2008), allowed us to test the effect
of unambiguous versus ambiguous acoustic inputs and the effect of predictable and
unpredictable contexts, on the neural encoding of pitch. Importantly, although the missing

fundamental has been shown to be restored perceptually, and potentially represented weakly in
brainstem auditory nuclei, at the level of the cochlea the two stimulus types are non-
overlapping: F0 is represented along the basilar membrane in pure tones, but not in MF tones,
even as a non-linear distortion product (Greenberg, 1980; Galbraith, 1994). However, the extent
to which these differing pitch cues have been processed or represented for perceptual
interpretation at the level of cortex is unclear. Using a decoding framework, we address three
questions: First, is pitch encoded differently for sounds with different spectral content (reflecting
the input), or is there a shared pitch representation (reflecting the percept)? Second, if there is a
shared neural representation, when and where is that representation generated? Third, when
acoustic pitch cues are ambiguous, how is the pitch representation affected by contextual
expectations?
360
361 *Evoked ROI activity*
362
Tones were presented in blocks corresponding to three different musical keys, in randomly
presented order or in scale order. The scale order condition is useful in ensuring a contextual
expectation for the next tone, but evoked representations of the low and high octave of the scale
may be difficult to interpret due to their position at the beginning or end of the scale sequence.
Thus, in Figure 2, we show evoked activity in four regions of interest (ROIs; Heschl's gyrus,
superior temporal gyrus, middle temporal gyrus, and postcentral gyrus) for the 8 scale degrees
of one of the musical scales (Eb Major), presented randomly. The three auditory ROIs were
selected *a priori*, as motivated by prior literature investigating pitch processing in auditory cortex
(Patterson et al., 2002; Hall and Plack, 2008; Wilson et al., 2009). The somatosensory ROI was
a data-driven inclusion, based on our observation of strong tone-evoked activity in this region.
We extract the ROI activity using the *aparc* parcellation.
374
During the window around M100-associated activity, average activation in right hemisphere
ROIs (Figure 2, right column) seems to increase with scale degree, which indicates a tonotopic,
F0-based organization in terms of amplitude. However, the left hemisphere shows comparable
amplitudes between the first and last scale degree (low Eb and high Eb; Figure 2, left column),
suggesting an effect of pitch chroma, or octave equivalence. This is in accordance with work
showing distinct mappings of pitch height (specific octave) vs. chroma (cyclical notes of a scale)
(Warren et al., 2003) and an underlying octave structure to tonotopy (Brosch et al., 1999;
Brosch and Schreiner, 2000). However, this left lateralization is novel, as octave-tuned voxel
clusters have been found mostly in the right hemisphere (Moerel et al., 2015), and bilateral
chroma sensitivity has been shown for complex, but not pure tones (Briley et al., 2012). The
postcentral gyrus appears to represent pitch in a similar way to auditory areas, which will be
discussed later.
387
388 *Individual decoding differences and reliability*
389
390 Before aggregating individual responses in our decoding analyses, we first look at individual
391 pitch decoding timecourses (Figure 3A). A general pattern emerged of performance peaking
392 within the first 100ms for pure and complex tones. The peak is much less pronounced for

393 ambiguous tones, but the pattern is consistent across subjects. There are, however, some
394 subjects that exhibit notable double peaks and others that do not seem to peak at all.
395

We next performed a principal components analysis (PCA) on these timecourses and plotted
the proportion of explained variance for the first 28 components (Figure 3B, left). For all tone
types, there was a pronounced 1-factor structure, with explained variance leveling off beyond
the first component. This means that much of the variance in individual responses could be
explained by the scaling of a single response profile. In addition, we measured the distribution of
maximum pitch decoding scores (Spearman correlations) for each tone type within the first
200ms following tone onset (Figure 3B, middle), as well as the time of each maximum score,
relative to tone onset (Figure 3B, right). Together, these show that although subjects varied in
their maximum decoding scores, the latencies of these maxima are highly consistent across
tone types.
406

Finally, we examined which MEG sensors contributed most to pitch decoding in the pure tones
condition for each subject (Figure 3C). We did this by extracting the Ridge regression weights
assigned to each sensor when decoding performance peaked, averaged across five folds of
cross-validation. The weights vary topographically by subject, but most show clusters of high-
contributing sensors in bilateral temporal regions, with the upper and lower halves of each
region showing opposite polarity. Taken together, these analyses suggest that there is variability
in the strength, but not the structure, of pitch encoding as derived from individual MEG activity.
414

415 *Decoding tone type*
416

Next, we tested at the group level whether pure and complex MF tones elicit distinct auditory
responses, given that their spectral content is different, but their fundamental frequency is the
same. To do so, we used a logistic regression classifier to distinguish between the pure and
complex MF 'tone types' (see Methods). We fit the classifier at each 5-millisecond time sample
separately, for each subject, using the activity across the 208 MEG channels for each epoch as
the input features. This resulted in a timecourse of decoding performance for each subject,
resolved at the 5-millisecond scale. Classifier performance was quantified using area under the
curve, which summarizes the similarity between the true stimulus labels and the classifier's
predictions of those labels. If the two signal types elicit the same neural response, the classifier
will be unable to provide an accurate label to distinguish the two classes, and so the decoding
performance should not differ from chance (AUC=0.5). If the two tones systematically elicit two
distinct responses, the difference in response will be learnable by the classifier, leading to
above-chance decoding performance. To evaluate statistical significance, we used a temporal
permutation cluster test (see Methods). This nonparametric approach controls for Type I error
by empirically testing the distribution of results that could have been obtained by chance and
comparing that to the observed result. The output is a series of time-windows that have been
evaluated for statistical significance. Given that the tone was played from 0 to 300ms, we used
a search window of -200 to 600ms, to investigate neural responses during the stimulus and
during the silence in between tones.
436

As shown in Figure 4A (left panel), tone type for pure versus complex MF tones could be
decoded significantly better than chance for almost the entire duration of the tone (-180-280ms,
df = 27; t = 5.2, p = 0.0001) as well as the silent period before the next tone (320-525ms, df =
27; t = 4.98, p = 0.0001). This suggests that spectral distinctions between acoustic inputs are
robustly encoded throughout the processing of the tone and are even maintained between
tones.

To determine the localization of the missing fundamental (MF) spectral distinction, we first
performed source localization on the MEG single trial epochs. This transformed the data from a
208-dimensional sensor space into a 5124-dimensional source space, with reconstructed
sources tiling the cortical surface. We then morphed the activity projected onto each subject's
MRI to a common template brain, to have the same source space across subjects. To
determine which of these localized sources encoded the spectral distinction between tone
types, we again used a decoding framework. Instead of fitting the logistic regression classifier
with the activity pattern across space at each millisecond, we instead fit the classifier with a
window timecourse of activity at each reconstructed source. This yielded a spatial map of AUC
scores, for each spatial source, for each subject.

We fit this decoder on the timecourse of activity in 50ms windows for the entirety of the epoch to
produce a spatial map of decoding performance across time (Figure 4). We found that the most
informative sources for distinguishing pure and complex MF tones throughout the entirety of the
tone and silent periods (Figure 4A) were in the auditory cortex, bilaterally within Heschl's gyrus
(df = 27, average t = 5.31, p < 0.001), superior temporal gyrus (df = 27, t = 5.4, p < 0.001) and
middle temporal gyrus (df = 27, average t = 4.27, p < 0.001), and in the sensorimotor cortex,
within the precentral gyrus (df = 27, average t = 3.19, p < 0.01) and postcentral gyrus (df = 27,
average t = 3.42, p < 0.001). Right hemisphere sources were more significant than left
hemisphere in superior temporal gyrus (df = 27; average t = 2.28, all p < 0.05) and postcentral
gyrus (df = 27; average t = 2.37, all p < 0.05) from 0-100ms and in Heschl's gyrus from 0-50ms
(df = 27; t = -3.15, p = 0.004). Tone type encoding in the postcentral gyrus was also right
hemisphere dominant between 250-350ms (df = 27; average t = 2.64, all p < 0.03). There was
no significant difference in tone type encoding between auditory and sensorimotor areas. This
suggests that pitch-invariant spectral envelope structure is encoded in neural populations
throughout the auditory and sensorimotor cortex, with a right-hemisphere dominance.

Finally, we sought to understand to what extent the neural responses to pure and complex MF
tones were distinguishable from the ambiguous tones, given that we created them as a
weighted mixture of acoustic cues. We fit the same logistic regression classifier described
above. Decoding performance for pure vs. ambiguous tones was similar to that of pure vs.
complex MF, with tone type being decoded significantly better than chance for the entire
duration of the tone, including the silent period after the tone (-170-590ms, df = 27; t = 4.80; p =
0.0001) (Figure 4B). Next, we trained a classifier to distinguish between complex MF and
ambiguous tones. Here, we found that tone type was decoded significantly better than chance
only for the duration of the tone (60-270ms, df = 27; t = 6.78, p = 0.0001), as well as a short
period directly before the beginning of the next tone (560-595ms, df = 27; t = 3.45, p = 0.01;

Figure 4C). This attenuated distinction between complex MF and ambiguous tones makes
sense, given that their spectral complexity and composition is similar compared to the pure
tones. Indeed, the ability to distinguish them at all is quite remarkable given the subtlety of their
acoustic difference.
485
We evaluated the spatial localization of these contrasts using the same decoding procedure we
applied for pure and complex MF tones. Interestingly, the localization of effects was similar, but
with sensorimotor area dominance. The distinction between pure and ambiguous tones
localized to auditory cortex and sensorimotor cortex. Heschl's gyrus encoded this distinction
only in the left hemisphere from -50-0ms (df = 27; t = 3.88, p = 0.0007) and from 150-300ms (df
= 27, average t = 3.24, all p < 0.01), but bilaterally otherwise (df = 27; average t = 4.14, all p <
0.01). Tone type was significantly encoded in bilateral superior temporal gyrus (df = 27, average
t = 3.81, all p < 0.01), middle temporal gyrus (df = 27, average t = 3.52, all p < 0.01), precentral
gyrus (df = 27, average t = 3.51, all p < 0.01) and postcentral gyrus (df = 27, average t = 3.81,
all p < 0.001). There was significantly higher decoding in sensorimotor areas than auditory
areas from -200-50ms (df = 27, average t = 3.5, all p < 0.01) and from 450-550ms (df. =27;
average t = 3.44, all p < 0.001).
498
The more subtle distinction between complex MF and ambiguous mixture tones localized to
bilateral sensorimotor cortex for the entirety of the tone and silent periods, with significant
decoding in precentral gyrus (df = 27, t = 2.98, p = 0.01) and postcentral gyrus (df = 27, t = 3.50,
p < 0.001). Tone type decoding in auditory areas was left hemisphere dominant during early
and later windows (-200-0ms, 350-600ms; df = 27; average t = 2.45, all p < 0.01) but bilateral
middle and superior temporal gyri encoded pitch from 0-350ms (df = 27; average t = 3.45, all p
< 0.0005). Heschl's gyrus encoding was significantly higher in the left hemisphere from 50-
100ms (df = 27; t = 2.35, p = 0.03) and left hemisphere dominant from 100-500ms (df = 27;
average t = 3.10, all p < 0.01). Decoding was more significant in sensorimotor areas than
auditory areas for all time windows except for 50-100ms (df = 27, average t = 2.47, all p < 0.03).
509
Although representing distinct information, the pre- and postcentral gyri are functionally
integrated, with regions of high connectivity linking somato-cognitive control and action (Gordon
et al., 2023). Our initial findings support the notion that pre- and postcentral gyri together may
comprise an important node of our auditory processing apparatus. The structure of responses in
motor cortex have been shown to represent acoustic features over articulatory features when
listening to speech sounds (Cheung et al., 2016), and melody and tempo discrimination tasks
have been shown to engage the postcentral gyrus specifically (Thaut et al., 2014). Additionally,
although often reflecting task-related motor processing, sound-related motor representations
have been found in SMA and pre-SMA during passive listening tasks and may represent
sensory predictive processing during auditory perception (Zatorre et al., 2007; Nastase et al.,
2014; Lima et al., 2016; Gordon et al., 2018). Differences between musicians and non-
musicians, as well as between those with and without absolute pitch, have been shown in
premotor areas, with musicians recruiting pre-SMA and SMA more than non-musicians during
music perception tasks (Grahn and Rowe, 2009; Margulis et al., 2009). Specifically relevant to
the distinction between ambiguous tones and pure/complex tones, sensorimotor cortex has

been implicated in the processing of timbre (Wallmark et al., 2018; Criscuolo et al., 2022).
Taken together, the initial pitch organization we find in evoked responses (Figure 2) as well as
the encoding of subtle spectral differences (Figure 4) are supported by these results.
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529
530 *Decoding pitch from distinct acoustic cues*
531
Having established that the responses to the three tone types are distinct, we next focused on
the encoding of pitch in each of the three tone types. We again used a decoding framework for
this. Because pitch is a continuous feature rather than a binary class, we used a ridge
regression model. Accordingly, we used Spearman rank correlation to summarize the similarity
between the true pitch values and predicted pitch values, given that they are both continuously
varying. Chance performance for a Spearman correlation is zero.
538
We performed the decoding analysis separately for each tone type and derived a timecourse of
Spearman correlation values for each subject. We then performed statistical analyses on the
distribution of decoding performance across subjects to test whether it was significantly different
from chance. Pitch decoding was significant for pure tones between 40 –165ms (df = 27; t =
5.67, p = 0.0001) and during the silent period between 245-595ms (df = 27; t = 3.25, p = 0.0001;
Figure 5B, left panel). This final period includes stimulus-related evoked activity, as well as the
silent period following each tone. For complex MF tones, pitch decoding was significant from 45-
300ms (df = 27; t = 4.8; p = 0.01) and from 410-450ms (df = 27; t = 4.07; p = 0.008; Figure 5B,
middle panel). Decoding performance peaked at 95ms for pure tones, and at 85ms for complex
MF tones. Overall, this result demonstrates that pitch is robustly encoded in neural responses to
the two spectrally non-overlapping tones.
550
Having established that two non-overlapping acoustic cues for pitch – F0 and inter-harmonic
spacing – lead to robust neural encoding of pitch along a similar timecourse, we next tested for
the encoding of pitch in the ambiguous tones. Although pitch is ambiguous, leading at times to
distinct percepts depending on context, we assigned pitch labels based on the lowest present
frequency, F0. Pitch was significantly decodable from -195 – -160ms (df = 27; t = 4.04, p =
0.02), 20-215ms (df = 27; t = 3.9, p = 0.0001) with notable a dip in decoding accuracy at 95ms,
365-395ms (df = 27; t = 2.9, p = 0.05), and 525 – 595ms (df = 27; t = 4.05, p = 0.0007; Figure
5B, right panel). Pitch was more weakly encoded in the ambiguous tones than the unambiguous
tones: decoding in pure tones was significantly higher from 80-115ms (df = 27; t = 5.75, p <
0.001), and decoding in complex MF tones was significantly higher from 65-110ms (df = 27; t =
5.26, p < 0.001). However, the ability to decode pitch from these tones suggest that the auditory
system settles on a pitch representation in the face of ambiguity, though weaker than that
evoked by unambiguous tones.
564
Next, we assessed the spatial localization of pitch encoding. We used the same procedure
described above, which was to estimate the decoding performance at each spatial source, for
50ms windows from -200 to 600ms. In pure tones (Figure 5A, left panel), pitch was encoded
between 0-50ms in the left postcentral gyrus (df = 27; t = -2.06, p = 0.05), with significantly

higher activity in sensorimotor areas than auditory (df = 27; t = 2.32, p = 0.03). Left Heschl's
gyrus significantly encoded pitch between 50-100ms (df = 27; t = 2.37, p = 0.03), and the right
superior and middle temporal gyri showed significant encoding from 50-150ms (df = 27; t = 3.39,
p = 0.005; df = 27; t = 2.89, p = 0.005). Heschl's gyrus showed pitch encoding in the 250-300ms
window (df = 27; t = 2.06, p = 0.05, with higher right hemisphere encoding during 300-350ms (df
= 27; t = -2.33, p = 0.03). There was higher sensorimotor area encoding than auditory from 350-
400ms (df = 27; t = 2.74, p = 0.01), with significant encoding in the left precentral and
postcentral gyri (df = 27; t = 2.12, p = 0.04; df = 27; t = -2.45, p = 0.02).

In complex MF tones (Figure 5A, middle panel), pitch was encoded between -100--50ms before
tone onset in left Heschl's gyrus (df = 27; t = 2.08, p = 0.05). Right Heschl's and middle
temporal gyri encoded pitch between 50-100ms (df = 27; t = 2.68, p = 0.01; df = 27; t = 3.93, p =
0.0006), with bilateral superior temporal gyrus encoding (df = 27; t = 2.09, p = 0.05; df = 27; t =
4.84, p < 0.0001). From 100-150ms, pitch was encoded bilaterally in Heschl's gyrus (df = 27; t =
3.46, p = 0.002) and in superior temporal gyrus (df = 27; t = 4.60, p = 0.0001). Similarly to pure
tones, there was higher sensorimotor area encoding than auditory in later windows, from 350-
450ms (df = 27; t = 3.32, p = 0.002; df = 27; t = 2.07, p = 0.05).

Ambiguous tone decoding showed a different pattern (Figure 5A, right panel), with pitch being
encoded -50-0ms before tone onset in left Heschl's and superior temporal gyri (df = 27; t = 2.44,
p = 0.02; df = 27; t = 2.09, p = 0.05), and right middle temporal gyrus (df = 27; t = 2.83, p =
0.009). From 0-50ms, right Heschl's gyrus encoded pitch (df = 27; t = 2.39, p = 0.02), pitch was
not significantly encoded in any ROIs from 50-100ms, and right Heschl's gyrus encoded pitch
from 100-200ms (df = 27; t = 2.17, p = 0.04, df = 27; t = 2.59, p = 0.02). Later windows were
dominated by sensorimotor areas, with significant pitch encoding in the right precentral gyrus
from 250-300ms (df = 27; t = -2.31, p = 0.03), bilateral precentral and right postcentral gyri from
400-450ms (df = 27; t = -2.70, p = 0.01; df = 27; t = -2.57, p = 0.02, and right precentral gyrus
from 500-550ms (df = 27; t = -2.63, p = 0.009). In sum, pitch encoding did not broadly alter its
spatial distribution across tone types, but it was significantly attenuated in the ambiguous tones,
mirroring the temporal decoding result. These findings suggest that pitch is robustly encoded in
response to isolated F0, isolated harmonic structure, and ambiguous mixtures of these two cues
leads to weaker pitch encoding.

Role of context in pitch encoding

So far, the results focused on the encoding of two acoustic cues for pitch: fundamental
frequency and inter-harmonic spacing. Next, we examine a third cue for pitch – expectation,
given a tonal context.

We presented the pure and complex MF tones to our participants in a scale (high expectation)
and random (low expectation) context. To assess the role of context for pitch encoding, we fit
separate decoders on these two contexts and re-ran the temporal decoding procedure (Figure
5C, left and middle panels). In pure tones, the mean t-value for all clusters was smaller than
1.96 (uncorrected p < 0.05), showing the difference in decoding performance for scale vs.

random context did not reach significance. In complex MF tones, decoding performance was
significantly higher overall for the random context as opposed to the scale context from 85-
115ms (df = 27; t = 3.52, p = 0.01).
616
Regarding pitch encoding outside the window of tone presentation, decoding performance
separated by scale vs. random context in pure tones showed that pitch was significantly
encoded before (-100 – -70ms; df = 27; t = 3.58, p = 0.04) and after (350 – 595ms; df = 27; t =
3.41, p = 0.0001) tone presentation when presented *in a scale context,* but not for tones
presented randomly. Similarly, pitch was significantly encoded after tone presentation (415 –
445ms; df = 27; t = 3.08, p = 0.04; 555 – 575ms; df = 27; t = 3.74. p = 0.04) for complex MF
tones presented in a scale context, but not when presented randomly. Thus, pitch encoding
before and after tone presentation, was limited to the stimuli presented in a scale, and may
reflect pitch prediction and maintenance during silent periods.
626
Next, we assessed the role of context for pitch encoding in the ambiguous tones, using the
same decoding procedure. Pitch ambiguity has been shown to be resolved in context (Deutsch
et al., 2008), so we created a high expectation condition: scales that end and begin on the same
octave-ambiguous tone. When applying the analysis to the high expectation scale condition, we
found that pitch can be decoded from -200 – -140ms (df = 27; t = 4.89, p = 0.004), 35-240ms (df
= 27; t = 4.38, p = 0.0001), and 515-595ms (df = 27; t = 5.56, p = 0.0002); when applied to the
low expectation random condition, pitch was encoded for a much shorter time period: from only
120 – 165ms (df = 27, t = 2.76, p = 0.003). We found that pitch could be decoded from the scale
condition significantly better than the random condition from 55 - 110ms (df = 27; t = 2.93, p =
0.002; Figure 5C, right panel). Overall, these results indicate that pitch is decodable earlier
when context is available as a cue to help derive the pitch percept of an ambiguous tone.
638
In sum, the outcome of our context analysis is that expectation only facilitates pitch encoding in
the cases where acoustic cues are ambiguous. In the pure and complex MF tones, the acoustic
cues are strong enough in pure/complex MF tones at their decoding peaks (85 vs. 95ms,
respectively) to derive pitch regardless of context. The result showing higher decoding
performance for complex MF tones in a random context is perplexing and requires further study
for a clearer interpretation. In ambiguous tones, where the cues are weak or contradictory, the
latency of pitch encoding is significantly modulated by context. High prediction scale contexts
lead to pitch being immediately extracted from the sensory input (earliest peak at 75ms);
whereas low prediction random contexts lead to pitch being extracted much later (earliest peak
at 130ms).
649
650 *Pitch generalization*
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The data establish that representations of pitch unfold along a similar timecourse and localize to
similar brain areas, when elicited by pure and complex MF tones, with weaker classification
performance in ambiguous tones. Next, we test whether this pattern is consistent with the
hypothesis that the neural coding scheme is shared across the two, or whether 'fundamental

frequency pitch' is represented in a distinct neural pattern of activity from 'inter-harmonic interval
pitch.'

To evaluate this, we trained a ridge regression model to decode pitch within one tone type and
evaluated how well that model was able to reconstruct pitch based on *responses to the other*
tone type. Given our observation that the peak in decoding performance differed between pure
and complex MF tones, it is possible that the neural processes that unfold for the two different
tone types are offset in time. To find the optimal alignment, we performed a temporal
generalization analysis (King and Dehaene, 2014), which allows us to find correspondences
between neural representations that may be temporally offset.

This analysis allows us to test different hypotheses regarding the representation of pitch across
tone types, and the relative latency with which pitch is derived in each case. These hypotheses
are visually presented in schematic Figure 6A. Of most importance is whether (i) there is any
generalization across tone types at all, and if so, (ii) with what relative latency difference.

To establish an interpretable baseline for comparison, we first performed temporal
generalization within each tone type (Figure 6B-C). As expected, there was robust decoding
throughout the tone, with strongest decoding along the diagonal whereby the neural activity
used to train the decoder best approximates the neural activity used to test the decoder.

Next, we applied the temporal generalization analysis *across* conditions. That is, we trained the
decoder on pure tones and evaluated decoding performance on complex MF tones, and vice
versa. This analysis revealed above-chance decoding that emerges earlier in complex MF tones
(~65-110ms, peaking at 80ms) than pure tones (~75-140ms, peaking at 95ms) (df = 27; p =
0.0008, t = 2.99; Figure 4D-E). This suggests there is a *shared pitch representation* – the same
neural pattern of activity encodes pitch across tone types – which is offset in time by ~10ms. We
use this optimal temporal alignment across tone type processing in subsequent
analyses. Although the biological significance of this time offset is unclear, the complex MF
tones acquire more pitch 'evidence' more quickly, as more neural ensembles are activated in
response to multiple spectral components. There may be a number of underlying neural
ensembles that give rise to this shared pattern.

Interestingly, although the initial pitch representation was shared across tone types during peak
decoding time, we found that the later encoding of pitch, for example during the silent period
between tones, did not generalize across conditions. This may suggest that while initial pitch
encoding is shared between acoustic cues, the later representation is specific to the acoustic
input that derived it.

Combining acoustic and contextual pitch cues

Next, we tested whether the neural representation of pitch in the ambiguous tones is also
shared with the pitch representation of the pure and complex MF tone stimuli, and whether this
representation is affected by contextual expectation. Again, because the processing lag

between stimulus types was not known *a priori*, we applied temporal generalization analyses,
whereby we fit ridge regression decoding models on the responses to pure tones, and
separately to complex MF tones, and then evaluated pitch decoding performance on the
ambiguous tones. To evaluate the effect of context, we fit our decoders separately on the tones
presented in a scale condition (providing high expectation contextual cues – "scale") and those
with random presentation order (low expectation contextual cues – "random").
706
First, we tested if pitch is represented for ambiguous tones in the most predictive scale context.
Our results revealed that the decoder, when trained on neural responses from 80-120ms to pure
tones, significantly generalized to the representation of pitch in ambiguous tones both from 20-
90ms (df = 27; t = 3.78, p = 0.0005) as well as from 125-180ms (df = 27; t = 3.51, p = 0.01).
There were two distinct decoding peaks, with decoding of pure tones at 95ms generalizing most
highly to ambiguous tones at 65ms (df = 27; t = 5.04, p < 0.001) and 150ms (df = 27; t = 4.45, p
< 0.001), as shown in Figure 7B, left. A similar result was found for the complex MF tones: the
pattern of neural activity from 60-105ms significantly generalized to ambiguous tones from both
15-90ms (df = 27; t = 3.86, p = 0.0006) and from 135-180ms (df = 27; t = 3.56, p = 0.0016). The
two decoding peaks are similar but shifted forward in time across the training dimension by
15ms: decoding of complex MF tones at 80ms generalized most highly to ambiguous tones at
65ms (df = 27; t = 5.42, p < 0.001) and 155ms (df = 27; t = 3.93, p < 0.001), as shown in Figure
7C, left.
720
721 These results support two findings. First, the neural representation of pitch is not only shared
722 between pure and complex MF tones but is also shared with ambiguous tones which contain a
723 combination of pitch cues. Second, unlike the processing of pitch in unambiguous pure and
724 complex MF tones, the pitch representation in ambiguous tones in context is maintained in
725 neural activity during distinct early and later windows *throughout the duration of the tone*.
726
Finally, we sought to understand how the neural representation of pitch emerges over time
when aiding context is removed for the ambiguous tone sequences. Interestingly, when applying
our analysis to ambiguous tones presented in a random context, we found that the neural
representation of pitch derived from pure tones during initial acoustic encoding at 90-120ms did
not emerge in neural responses to ambiguous tones until 145-160ms (Figure 7B, right; df = 27; t
= 3.54, p = 0.038). Decoding of pure tones at 100ms generalized with the highest performance
to random ambiguous tones at 145ms (df = 27; t = 4.06, p < 0.0001). The neural representation
of pitch derived from complex MF tones at 75-95ms generalized to 135-160ms (Figure 7C, right;
df = 27; t = 4.03, p = 0.019). Decoding of pure tones at 90ms generalized with the highest
performance to ambiguous tones at 140ms (df = 27; t = 5.35, p < 0.0001). In other words,
whereas in the scale presentation pitch is encoded from 20-90ms, when the same tones are
presented in a random order, the same pitch cues are encoded, but not until 130-180ms. This
suggests that in the case where the acoustic cues are ambiguous, any context serves to
generate an initial pitch representation, which is absent in the case where context is unreliable
or considerably weaker.
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We complement this generalization analysis by plotting pitch source decoding results within
ambiguous tones for the two windows in which pitch generalized from pure and complex MF
tones to ambiguous tones (50-100ms and 150-200ms), for each context (Figure 7A). This
demonstrates a lack of any pitch representation in the early window (50-100ms) for randomly
presented ambiguous tones, in contrast with representations of pitch in both the early and later
window for ambiguous tones presented in a scale context.
749
750 **DISCUSSION**
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This study investigated how acoustic and contextual cues are cortically processed and
integrated to facilitate pitch perception. We created stimuli that cued pitch via unambiguous
fundamental frequency, unambiguous inter-harmonic intervals, and an ambiguous mixture, and
we placed those signals in high and low expectation contexts. The time-resolved neural
decoding approach we use provides a new analytic methodology to assess different possible
representational schemes in the processing and representation of pitch.
758
We first address whether is pitch encoded differently for sounds with different spectral content
(reflecting the input), or whether is there a shared pitch representation (reflecting the percept).
Overall, we find that pitch is robustly encoded in neural responses to each tone *type* (consistent
with the literature), and that the representation is shared between different acoustic and
contextual cues. This unified pitch representation emerges at different latencies, however,
depending on the acoustic cues available as well as the strength of the supporting context.
765
We then address when and where this shared representation is generated. The two acoustic
cues for pitch appear to converge on the same representation in cortex, predominantly
localizing to the right superior and middle temporal gyrus and surrounding auditory areas. Given
the limitations of source localization accuracy with MEG, it is possible that the responses we
observe in the middle temporal gyrus emerge from a bleeding over of activity from the auditory
cortex. This is supported by the observation that the pattern of evoked responses is qualitatively
similar across these ROIs (see Figure 2). This dominance of pitch representations in the right
hemisphere is broadly in accordance with other work (Zatorre and Belin, 2001; Zatorre et al.,
2002; Jamison et al., 2005; Hyde et al., 2008; Zatorre, 2022). Recent studies using lesion
network mapping have confirmed right temporal and subcortical areas as crucial neural
substrates for music processing, and more specifically, detecting fine pitch differences
(Sihvonen et al., 2016; Sihvonen et al., 2024). This hemispheric asymmetry may be driven by
differences in local *spectral* or *temporal interconnectivity patterns* in auditory cortex between the
right and left hemisphere, respectively (Obleser et al., 2008; Cha et al., 2016). This bottom up,
or, input-driven, specialization, however, has been shown to interplay with top-down
mechanisms, such as perceptual categorization (Tierney et al., 2013), learning (Dehaene-
Lambertz et al., 2005; Möttönen et al., 2006), and selective attention (Brodbeck and Simon,
2022). However, pitch is not completely absent from the left hemisphere, suggesting that there
are pitch-encoding neural populations bilaterally (Allen et al., 2017; Zatorre, 2022). Given the
simplicity of the auditory signals used to elicit pitch percepts in this study, low-level temporal
information relating to pitch may still be encoded in left auditory regions, to be integrated with

top-down information later in the processing stream. Interestingly, while we found that the distinction between pure and complex MF tones was right lateralized, the distinction between both unambiguous tone types and ambiguous tones was bilateral, if not slightly left lateralized. This distinction was also most prevalent in sensorimotor areas, which has not been shown before. The relevance of sensorimotor cortex in distinguishing between subtle differences in spectral information remains to be explored.

Although the data suggest that the neural representation of pitch recruits the same neural populations across pitch cues, we found that these populations peaked significantly earlier for complex MF tones (~85ms) than pure tones (~95ms). This could be attributed to the fact that the complex MF tones contain higher-frequency spectral content, with spectral centroids closer to the shortest-latency ~1 kHz response of neurons in auditory areas (Roberts and Poeppel, 1996; Roberts et al., 1998). Although this difference is small, is supported by work showing that both F0 and pitch height, i.e. the spectral envelope, influence the latency of the pitch response (Ritter et al., 2007; Sauvé et al., 2021). Alternatively, the latency difference we observe could be due the fact that the higher frequencies provide a larger number of completed frequency cycles (i.e. more evidence) in order to derive a frequency estimate (Gage and Roberts, 2000), or to pitch being faster to compute based on harmonic interval cues than fundamental frequency based on the acoustic cues available from the periphery. The mechanistic origin of the latency difference we find merits further targeted investigation.

Lastly, we explored how the pitch representation is affected by contextual expectations. We found that when the acoustic cues for pitch are clear and unambiguous, there is little effect of context, in either the strength of pitch encoding or its latency. In fact, we found a slight increase in pitch encoding in the random context for complex MF tones, which may be explained under a predictive coding framework, whereby the higher prediction error generated by randomly presented tones leads to stronger pitch representations. For ambiguous signals, however, we found that context played a major role in adjusting the dynamics of pitch processing. Concretely, pitch was decodable with a peak around 80ms when presented in a predictable context and around 120ms when presented in a random context. The immediacy of pitch representation in predictable contexts suggests that the *expectation* of pitch is instantly integrated with — or used to directly bias the processing of — the impoverished acoustic cues. This result fits with recent work showing that context does not necessarily enhance the pitch representation itself, but rather primes the auditory system for expected stimuli (Graves and Oxenham, 2017). Thus, the pitch of ambiguous tones was more easily accessible earlier when presented in context, but a similarly strong pitch representation still emerged, albeit later, without context. Listening context, as opposed to the presence of a tonal hierarchy, may play a more direct role in *enhancing sensitivity* to pitch (Garcia et al., 2010). This result also supports the mechanism of auditory prediction signaling, in which target predictions are encoded in auditory cortex (Chouiter et al., 2015; Berlot et al., 2018). Whether predictions are propagated down from higher cortical areas or up from subcortical activity remains to be elucidated. In addition to showcasing the importance of expectation in pitch processing, the influence of context on acoustically identical sounds demonstrated here also highlights the dynamic flexibility of the processing system and the ability to integrate different cues, at different times, depending on the information available.

The findings we report show that different cues for pitch, including acoustic and contextual
information, converge on a shared neural representation that is normalized for differences in
spectral content and expectation. In naturalistic settings, pitch will likely be derived by combining
information across multiple cues, some weak and some strong. Our results indicate that
regardless of the specific cues used to generate a pitch percept, the representation converges
on a common activity pattern in right-lateralized superior temporal gyrus. This finding supports
the existence of a pitch-processing center (Patterson et al., 2002; Krumbholz et al., 2003;
Bendor and Wang, 2005; Chait et al., 2005). However, this does not preclude the presence of
other frequency- or timbre-based representations throughout auditory cortex – high decoding of
pitch *within* (but not across) tone types specifically during later time windows suggests spectrally
specific tonotopic representations downstream (Allen et al., 2022). Importantly also, we did not
fix the spectral bandwidth across stimulus types, as our interest was in comparing orthogonal
cues to pitch. Thus, in our stimuli, not only does the musical pitch get modulated up and down
the scale, but the spectral content (harmonics) is also shifted within the same range (one
octave). Thus, decoding performance may reflect this relative spectral shift in addition to pitch.
Additionally, high decoding of tone type (pure vs. complex MF), suggests the existence of a
timbre-sensitive region within both auditory and sensorimotor cortex (Bizley et al., 2009; Allen et
al., 2017). Similar analyses could be applied to an exploration of absolute vs. relative pitch
encoding and the role of pitch for different auditory domains, such as melodic and speech
processing.

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Figure 1. Experimental stimuli. (A) Tone types. Waveforms, spectral content, and perceived pitch for a pure tone, complex missing fundamental (MF) tone, and ambiguous tone of 220Hz. **(B) Evoked responses.** MEG evoked responses (and topoplots) across all sensors averaged across participants, for each tone type. **(C) Musical keys.** Musical notation for each of the three scales used to create stimuli. **(D) Harmonic components.** Harmonic components for each scale degree of one example scale (A major) for each stimuli type. Pure and complex MF tones contain flat amplitudes across harmonics, while ambiguous tones contain differently attenuated harmonics for each scale degree.

Figure 2. Evoked ROI activity. MEG activity averaged across all trials and all participants for the 8 scale degrees of the Eb Major scale, tones presented randomly. Activity is plotted in the left *(left column)* and right *(right column)* hemisphere for four ROIs: transverse temporal (Heschl's) gyrus **(A)**, superior temporal gyrus **(B)**, middle temporal gyrus **(C)**, and postcentral gyrus **(D)**. Bar plots show average activity within three temporal windows after tone presentation: 30-70ms *(left bar plot)*, 90-130ms *(middle bar plot)*, and 160-240ms *(right bar plot)*.

Figure 3. Individual differences and reliability of decoding. (A) Individual decoding performance for pure tones *(left),* complex MF tones *(middle),* and ambiguous tones *(right).* Each row represents one participant, which are ordered by maximum decoding performance across the three tone types. **(B)** Principal components for each decoding timecourse *(left)*; Distribution of maximum decoding scores, plotted as a histogram with bin width 0.006, for each tone type. This is overlaid with a Gaussian kernel density estimator (KDE) approximation with bandwidth selected via Scott's method (Scott, 1992) *(middle)*. Latency of max Spearman R, plotted with a bin width of 20, overlaid with a Gaussian KDE to select bandwidth *(right)*. **(C)** Feature importance sensor maps for all participants for pure tone decoding, plotted as Ridge regression weights for each sensor at decoding peaks averaged across five folds of cross-validation.

Figure 4. Tone type decoding. Decoding performance over time is plotted with standard error of the mean for each combination of tone types: pure vs. complex MF *(top)*, pure vs. ambiguous *(middle)*, and complex MF vs. ambiguous *(bottom)*. Temporal clusters of significant above-chance decoding (AUC) are shown shaded under the curve. Stimulus waveforms are depicted below each timecourse to denote tone duration. Source decoding of tone type averaged across 50-150ms after tone onset is shown for each tone type comparison. Colorbar denotes AUC values for each source.

Figure 5. Pitch decoding. (A) Source space decoding of pitch averaged across selected 50ms windows. Colorbar denotes Spearman R values for each source. **(B)** Decoding performance over time plotted with standard error of the mean for each tone type: pure *(left)*, complex MF *(middle)*, and ambiguous *(right)*. Temporal clusters of significant above-chance decoding (Spearman correlation) are shown shaded under the curve. Stimulus waveforms are depicted below each timecourse to denote tone duration. **(C)** Decoding performance for pitch in tones within context (scale, solid line) and out of context (random, dotted line) for each tone type. Shaded areas show standard error of the mean (SEM). Bars below show significant above-chance decoding clusters (Spearman correlation).

Figure 6. (A) Schematic of across-condition temporal generalization results under different neural hypotheses (top panel). If the neural pattern is distinct between conditions, at all latencies between conditions, we should observe no above-chance decoding at any train/test time pair. By contrast, if two conditions evoke shared neural representations, and that neural pattern is generated at the same latency across conditions, we will observe above-chance decoding performance along the diagonal, where training time is equal to testing time. If the same neural pattern is generated earlier in the test set as compared to the training set, we will observe above-chance decoding performance above the diagonal line. By contrast, if the same neural pattern is generated later, above-chance decoding performance will be below the diagonal. Finally, if the same neural pattern is generated transiently in the training set (e.g., pure tones), but maintained over time in the test set (e.g., we will observe above-chance decoding that begins at the diagonal and continues throughout test time. **Temporal generalization decoding for pitch within and across tone types (bottom panel). (B)** Decoding performance along the diagonal for pitch within pure tones and complex MF tones separately is plotted with standard error of the mean *(left)*. Stimulus waveforms are depicted below each timecourse to denote tone duration. **(C)** Temporal generalization results for a model trained (y-axis) and tested (x-axis) on pure tones *(left)* and trained (y-axis) and tested (x-axis) on complex MF tones *(right)*.

Contours delineate t-value thresholds of 2 (gray dotted line) and 3 (black dotted line). **(D)** Decoding performance
along a time-warped diagonal to adjust for latency differences in pitch decoding for a model trained on pure tones and
tested on complex MF tones (red line) and vice versa (blue line; *left*). Stimulus waveforms are depicted below each
timecourse to denote tone duration. **(E)** Temporal generalization results for a model trained (y-axis) on pure tones
and tested (x-axis) on complex MF tones (*middle*) and trained (y-axis) on complex MF tones and tested (x-axis) on
pure tones (*right*). Contours delineate t-value thresholds of 2 (gray dotted line) and 3 (black dotted line).

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Figure 7. Temporal generalization for decoding pitch in ambiguous tones. (A) Source decoding for ambiguous
tones in scale context (left) or random context (right) for the two windows in which pitch decoding from pure and
complex tones are shown to be significant. **(B)** Temporal generalization results for decoding pitch from ambiguous
tones presented in a *scale context* when trained on pure tones (left) or complex MF tones (right). Contours delineate
a t-value threshold of 3 (thin black line). (**C**) Temporal generalization results for decoding pitch from ambiguous tones
presented in a *random context* when trained on pure tones (left) or complex MF tones (right).

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C

Middle Temporal Gy

D

Postcentral G

Pure tones

A

Distinct processes

Condition 1 Training Time

n.s.

Testing Time
Condition 2

Shared processes

same latency

earlier

shift earlier

later

shift later

Condition 1 Training Time

Testing Time
Condition 2

B

Decoding Pitch: **within** tone type

Spearman R

— Pure
— Complex MF

Time (s)

C

Train Pure, Test Pure

Train Complex MF,

Training Time (s)

Testing Time (s)

Training Time (s)

Testing T

D

Decoding Pitch: **across** tone type

Spearman R

— Pure-Complex MF
— Complex MF-Pure

Time (s)

E

Train Pure, Test Complex MF

Train Complex

Training Time (s)

Testing Time (s)

Training Time (s)

Testing T