Functionally Adaptive Structural Basis Sets of the Brain: A Dynamic Fusion Approach

Marlena Duda[1] (mduda@gsu.edu), Jiayu Chen[1] (jchen84@gsu.edu), Aysenil Belger[2]

(aysenil_belger@med.unc.edu), Judith Ford[3,4] (Judith.Ford@ucsf.edu), Daniel Mathalon[3,4]

(Daniel.Mathalon@ucsf.edu), Adrian Preda[5] (apreda@uci.edu), Jessica Turner[6]

(jessica.turner@osumc.edu), Theo Van Erp[7,8] (tvanerp@hs.uci.edu), Godfrey Pearlson[9],

(Godfrey.Pearlson@hhchealth.org), Vince D. Calhoun[1,10] (vcalhoun@gsu.edu)

[1]Tri-Institutional Center for Translational Research in Neuroimaging and Data Science (TReNDS),

Georgia State University, Georgia Institute of Technology, and Emory University, Atlanta, GA 30303,

USA

[2]Department of Psychiatry, University of North Carolina, Chapel Hill, NC, USA

[3]Mental Health Service, San Francisco Veterans Affairs Healthcare System, San Francisco, CA, 94121,

USA

[4]Department of Psychiatry and Weill Institute for Neurosciences, University of California San Francisco,

San Francisco, CA, 94143, USA

[5]Department of Psychiatry and Human Behavior, University of California Irvine, Irvine, CA, 92697, USA

[6]Department of Psychiatry and Behavioral Health, Wexner Medical Center, The Ohio State University,

Columbus, Ohio, 43210, United States

[7]Clinical Translational Neuroscience Laboratory, Department of Psychiatry and Human Behavior,

University of California Irvine, Irvine, CA, 92697, USA

[8]Center for the Neurobiology of Learning and Memory, University of California Irvine, Irvine, CA,

92697, USA

[9]Departments of Psychiatry and Neuroscience, Yale University School of Medicine, New Haven,

CT, USA

[10]Departments of Psychology and Neuroscience, Georgia State University, Atlanta, GA, 30302, United

States

Abstract

The precise relationship between brain structure and function has been investigated through a multitude of lenses, but one detail that is held constant across most neuroimaging studies in this space is the identification of a singular structural basis set of the brain, upon which functional activation signals can be reconstructed to examine the linkage between structure and function. Such basis sets can be considered "functionally independent", as they are derived through structural data alone and have no explicit association to functional data. Recent work in multimodal fusion has facilitated a more integrated view of structure-function linkages by enabling the equal contribution of both modalities to the joint decomposition, resulting in components that are independent within modality but co-vary closely across modalities. These existing symmetric fusion approaches thus identify structural bases given an associated functional context. In this work we consider an additional layer of precision to the investigation of structure-function coupling by studying these context-dependent linkages in a time-resolved manner. In other words, we ask which features of brain structure become (or remain) salient given the dynamically changing functional contexts (i.e., dynamic functional connectivity states, task structure, etc.) the brain may pass through during a given fMRI scan. We introduce "dynamic fusion", an ICA-based symmetric fusion approach that enables flexible, time-resolved linkages between brain structure and dynamic brain function. We show evidence that temporally resolved, and functionally contextualized, structural basis sets can accurately reflect dynamic functional processes and capture diagnostically relevant structure-functional coupling while detecting nuanced functionally-driven structural components that cannot be captured with traditionally computed structural bases. Lastly, differential analysis of component stability across repeated scans from a control cohort reveals organization of static and dynamic structure/function coupling falls along unimodal/transmodal hierarchical lines.

Introduction

Over the last 50 years, advances in neuroimaging have produced a host of techniques capable of capturing detailed signatures of brain structure and function. Along with its potential for precision diagnostics in psychiatric and neurological conditions, the rise of neuroimaging has been instrumental in furthering investigation into one of the most fundamental questions in neuroscience: what is the relationship between brain structure and function? To this end, a class of approaches have been developed under the umbrella known as multimodal fusion, which aim to optimally integrate complementary data across various neuroimaging modalities. Multimodal fusion spans a wide range of techniques capable of revealing hidden linkages between imaging data types, and these techniques can be broadly divided into two categories: asymmetric fusion approaches, wherein data from one modality are used to constrain or

influence the analysis of another modality, and symmetric fusion approaches, wherein each imaging

modality contributes equally to the combined analysis, fully leveraging the joint information across

datasets (V. D. Calhoun & Sui, 2016; Sui et al., 2012).

In utilizing symmetric multimodal fusion to study the coupling between brain structure and function,

there arises the common challenge of dealing with dimensional incongruence between "static" measures

of brain structure and functional neuroimaging datatypes that include an additional temporal dimension.

Historically, this has been addressed by heavily summarizing over the temporal dimension of the

functional time series by computing measures such as static functional network connectivity (sFNC)

(DeRamus et al., 2022) or amplitude of low-frequency fluctuation (ALFF) (Lottman et al., 2018), which

does achieve dimensional compatibility of the data types for fusion, but also effectively removes the rich

temporal information of the functional data. Some data driven approaches including parallel ICA (Vergara

et al., 2014) group ICA + ICA (Qi et al., 2022) have been developed to handle mismatched data

dimensionality, however these have not yet been expanded to fully leverage functional dynamics. With

the surge in focus on functional dynamics over the last decade, the field has begun to recognize the

significance of short-scale variation in connectivity (particularly during rest) and has pushed to preserve

more temporal information in the analysis of fMRI data. A common output of dynamic functional

network connectivity (dFNC) analysis is the identification of a small set of dFNC states or patterns that

subjects may transition within and between during rest, often derived via k-means clustering (Allen et al.,

2014). Several multimodal fusion studies have operated on the level of dFNC states by concatenating

subject-level average connectomes across all states into a single FNC "mega-vector" in the fusion design

(Abrol et al., 2017; Duda et al., 2022), thus enabling the inclusion of dynamic information into the

multimodal fusion without increasing dimensionality of the functional inputs. Symmetric fusion

approaches, such as multiset canonical correlation analysis with joint ICA (mCCA + jICA), were then

applied to find hidden linkages between the concatenated dFNC and structural data, and functional

patterns specific to each dFNC state were reconstructed post-hoc. While this approach enables some

interpretation of state-specific linkages to structure, the resultant couplings are rather rigid as the

concatenated dFNC components necessarily share a single loading parameter linking to a single structural

component, imposing the (likely too strict) assumption that linkage to structure is identical across all

dFNC states. Other joint approaches have investigated functionally informed structural basis sets (Plis et

al., 2018) as well as individual linkages between specific intrinsic functional networks and structure

(Khalilullah et al., 2023), but thus far there has been no framework for systematically identifying flexible

structural basis sets based on linkages to time varying brain function.

On the flip side, widely used asymmetric fusion approaches are not bound by the same dimensionality

constraints as symmetric fusions, at the cost of being less informative about the joint relationship between

modalities. One particular line of research that has recently emerged and can be classified under the

umbrella of asymmetric fusion is the study of "structural brain modes". In short, structural graphs (which

can be derived as white matter structural connectivity matrices via tractography analysis on diffusion MRI

(Griffa et al., 2022) or maps of cortical surface geometry (Pang et al., 2023)) are subjected to eigenmode

decomposition to obtain a singular structural basis set representing the so-called "structural harmonics" of

the brain. These structural modes can be linked to brain function by projecting the fMRI signal at each

timepoint as weights onto the discovered structural manifold. Such an approach does enable some

flexibility in the linkage of structure to function over time through modification of the weighted mixture

of the structural modes, however the rigid definition of only one structural basis set derived without

explicit linkage to functional data assumes that the full realm of complex brain functions can be

sufficiently described by a singular set of structural modes.

It has long been known that functional brain activity and connectivity vary meaningfully over both long

(across the lifespan) (Battaglia et al., 2020; Baum et al., 2020) and short (seconds to minutes) (V. Calhoun

et al., 2010; V. D. Calhoun et al., 2014; Chang & Glover, 2010; Lurie et al., 2020; Preti et al., 2017)

timescales, however the potential for similar temporal variation in structure-function couplings, especially

at shorter timescales, has thus far been understudied. Most prior work has focused on either regional

(Fukushima et al., 2018; Fukushima & Sporns, 2020) or temporal (Preti & Van De Ville, 2019; Vázquez-

Rodríguez et al., 2019) fluctuations in structure-function coupling, but attempting to study simultaneous

spatiotemporal fluctuation patterns of structure-function linkages is a relatively novel concept. One such

work utilized multilinear regression to link regional measures of instantaneous functional connectivity to

their structural connectivity profiles derived from diffusion MRI (dMRI) as an estimate of time- and

region-resolved structure-function coupling (Liu et al., 2022). This study found that dynamic coupling

patterns reflect cortical hierarchies, showing the strongest spatiotemporal fluctuations in the insula and

frontal eye fields and the least in the unimodal and transmodal cortices. This atlas-based approach

represents a critical initial dive into the space of temporally-evolving structure-function coupling at the

level of data integration, and continued investigation into this space with advanced approaches like

multimodal fusion promises to yield even deeper insights in this emerging domain of research by enabling

joint estimation of data-driven structure-function linkages at the voxel level.

Here, we introduce an ICA-based symmetric fusion approach that allows for the identification of a

temporally adaptive basis set that is inclusive of both structure and function, which we term "dynamic

fusion". We wish to be explicit in the fact that we **do not claim** that neuroanatomical structure is
physically changing on short timescales. Rather, we explore the concept that a single basis set derived
from structural data alone may not provide the best representation of the highly complex interplay of
brain structure required for the full range of human brain function. We advocate for the creation of
structural features (i.e. basis sets/latent representations) in a way that is informed by the dynamically
changing functional contexts that individuals oscillate through across the duration of a functional scan.
Consider, as an intuitive example, the swinging pendulum system. The system has finite set of physical
properties that are unchanging during the observation period (akin to the structural properties of the brain
that are unchanging during the course of an MRI scan); however, depending on the functional aspect of
interest in the model (e.g., oscillatory motion or energy dissipation), different physical (i.e. "structural")
aspects of the system are required (e.g., angular position, angular velocity and pendulum length for
oscillatory motion, and velocity, surface area, coefficient of drag and friction at pivot for energy
dissipation), and thus different structural basis sets are defined for the same system. In the same way, our
dynamic fusion approach derives multiple structural basis sets for the same physical brain system that are
each best suited to describe the different functional "states" considered across time. In other words, what
we derive are temporally evolving patterns of structure-function *coupling*, rather than short-scale changes
in physical brain structure itself.
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The following paper highlights three key results. First, inter-state cross-fusion comparisons revealed that
structural components exist on a spectrum from high to low cross-fusion stability, which can be
interpreted as less functionally influenced (i.e., "static") to more functionally influenced (i.e., "dynamic").
Second, we show dynamic structural components exhibit the strongest group differences in component
loading parameters in a schizophrenia (SZ) vs. control cohort. Third, we show that the organization of the
brain into regions of highly static vs. highly dynamic structure-function coupling largely falls along
unimodal/transmodal hierarchical lines. These results indicate that dynamic fusion enables flexible
linkages between structure and time-evolving function which are related to changing cognitive demands,
and suggest that the functionally influenced dynamic components may capture clinically relevant
structure-function linkages that would be otherwise missed by standard approaches. In addition to
fMRI/sMRI fusion experiments, we show similar results with dMRI as structural inputs to the dynamic
fusion pipeline indicating measures of both white and gray matter show evidence for time-varying
coupling to function.
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Methods

Data & Preprocessing

We analyzed functional, structural, and diffusion MRI from the HCP 1200 (Van Essen et al., 2013) (N = 833 subjects, average age = 28.7 years) and FBIRN (Keator et al., 2016) (N = 310 subjects, N_{SZ} = 150 subjects [114 male, average age = 38.8 years], N_{CON} = 160 subjects [115 male, average age = 37.0 years]) datasets. All data were collected with informed consent and approved by the Institutional Review Boards at the participating institutions. Processing pipelines are detailed below:

fMRI: In both datasets, resting state fMRI data were preprocessed with a standard pipeline that included brain extraction, slice timing, and motion correction steps. Preprocessed data were then registered into structural MNI space, resampled to 3mm^3 isotropic voxels, and spatially smoothed using a Gaussian kernel with a 6mm full-width-at-half-maximum (FWHM) on a per-subject basis. Spatially constrained ICA was applied using the GIFT toolbox (https://trendscenter.org/software/gift/) (Iraji et al., 2021) using the NeuroMark_fMRI_1.0 template (Du et al., 2020) to extract subject-level spatial maps and for each of the 53 intrinsic connectivity networks (ICNs) defined in the template, as well as their respective activation time courses. Dynamic FNC (dFNC) analysis of fMRI differed between the HCP and FBIRN datasets in an effort to explore consistency of the results of our dynamic fusion approach relative to upstream pipeline design choices.

In FBIRN, time and frequency resolved FNC patterns were computed from ICN time courses using the filter-bank connectivity (FBC) approach (Faghiri et al., 2021). Briefly, FBC utilizes a filter bank, i.e., an array of systems used to filter a time series into different frequency bands (typically non-overlapping and spanning the full frequency spectrum of the data), which enables estimation of FNC within a given frequency range. We designed our filter bank to contain 10 Chebyshev type-2 infinite impulse response filters that evenly cover the full frequency spectrum of the fMRI time series (0.00 – 0.25 Hz). K-means clustering identified six distinct states with unique connectivity signatures and spectral occupancy across frequency bands. For more detail on the FBC approach and state clustering used here see (Duda et al., 2022).

In HCP, we utilized the REST1_LR and REST2_LR fMRI time series to perform repeated experiments within the same subject set and scan type. We computed dFNC in resting state fMRI from ICN time courses using a sliding window Pearson correlation (SWPC) approach outlined in (Damaraju et al., 2014), with the exception that the window size used in our analysis was 10 TR (~15s; TR = 0.72s). We chose a

10 TR window to keep consistency between the window size in HCP and FBIRN analyses. K-means

clustering in resting state data revealed five dFNC states, and subject-average connectomes were

computed for each state for dynamic fusion.

sMRI: All structural data were preprocessed using statistical parametric mapping (SPM12) under

the MATLAB 2019 environment. Structural images were segmented into gray matter, white matter, and

CSF using the modulated normalization algorithm. The gray matter volume (GMV) map outputs were

smoothed using a Gaussian kernel with FWHM = 10mm.

dMRI: The processing of dMRI data in HCP involves a series of steps using FSL

(www.fmrib.ox.ac.uk/fsl), ANTs (Avants et al., 2009), and custom-built software. First, the datasets were

collected with phase reversed blips, resulting in images with distortion in opposite directions. To address

it, volumes containing b0 (b=5, with phase encoding in the left-right (LR) and right-left (RL) direction)

were extracted from the entire set of 576 volumes for each dataset (comprising 3 LR runs with 95, 96 and

97 directions respectively, and 3 RL runs with corresponding directions). These b0 volumes were

preselected by identifying the least-distorted pair, which was then used with topup (FSL 6.0)(Andersson

et al., 2003) to estimate the susceptibility-induced off resonance field. The estimated fieldmap was used to

unwarp the phased-encoded dMRI images. Next, the dMRI volumes underwent correction for eddy

current distortions and head movement using eddy_gpu (FSL 6.0), which incorporated advanced motion-

induced signal dropout detection and replacement (Andersson & Sotiropoulos, 2016). Subsequently,

Fractional Anisotropy (FA) maps were estimated from the diffusion tensor model using dtifit (FSL 6.0).

The FA maps then underwent automated noise inspection, where any detected noise spots were padded

with interpolation, and all FA values were adjusted to fall within the range of 0 to 1. Following this, the

FA maps were registered to the Montreal Neurological Institute (MNI) standard space through nonlinear

registration performed by ANTs. Any images exhibiting excessive motion, signal dropout, or excessive

noise were excluded from subsequent analysis (Geenjaar et al., 2023; Wu et al., 2015).

Dynamic Fusion

We used multi-set canonical correlation analysis followed by joint independent component

analysis (mCCA + jICA) to perform fusion of both static (GMV/FA maps) and temporally resolved

(SWPC/FBC states) neuroimaging features. The combined mCCA + jICA model is designed to allow for

the identification of both strongly and weakly correlated joint components that are also independent from

one another. This is achieved by employing mCCA in the first step to generate flexible linkages between

the modalities, and subsequently applying jICA to ensure independence between components. The ability

to identify flexible (i.e., both strong and weaker) linkages between modalities is essential for the

application to dynamic fusion, in which we are searching for nuanced differences in the joint information

between structure and dFNC as a function of time, thus this requirement informed our design choice of

employing mCCA + jICA as the symmetric fusion algorithm. The mCCA + jICA framework is defined

under the assumption that a multimodal dataset, X_k, is a linear mixture of m sources (Sk) mixed by non-

singular matrices (A_k), here, k = (1,2). The effective mCCA + jICA framework can be defined as $X_k =$

$(D_k W^{-1})S_k$, where modality-specific mixing matrices are defined as $A_k = D_k W^{-1}$. Further details can be

found in (Sui et al., 2011, 2013).

The key novelty in dynamic fusion is the concept of performing multiple data fusions which are linked

together. In short, dynamic fusion generates functionally adaptive basis sets of brain structure by

conducting multiple fusion experiments linking a static neuroanatomical measure (e.g., GMV map) to

various distinct functional measures that represent temporally evolving functional patterns (Fig 1). This

can in theory be applied at various levels of functional granularity, but since resting state time courses are

not temporally aligned across subjects, window-level dynamic fusion would not be appropriate as the

underlying functional contexts/cognitive processes would not be fixed across subjects within each fusion.

Thus, to enforce some level of temporal and functional alignment in the resting state fMRI experiments,

we perform state-level dynamic fusion wherein structural measures (either GMV or FA maps) are

separately fused with subject-level state-average FNC matrices. All dynamic fusion experiments resulted

in a set of structural (GMV or FA) components (model order = 15) optimized to each time-resolved FNC

pattern independently. Cross-fusion comparisons of these structural components across experiments

revealed structural manifolds unique to each distinct functional basis (i.e., GMV/FA components related

to frequency-specific functional connectivity dynamics), as well as some that were identified across

multiple fusions, indicating a "static" structural component. In addition to the state-level fusion

experiments, we conducted intra-state (i.e., same-state) cross-fusion analyses to serve as baselines. For

each subject, timepoints corresponding to each dFNC state were randomly split into two equal sets and

subject-level average FNC was computed using the only the timepoints in each set. Each split-half FNC

matrix was used as a functional input to separate fusions and cross-fusion correspondence was computed

between fusions from the *same* state, thus assessing component stability across fusions where the

functional inputs were not identical but derived from the same functional context.

Fig 1. Schematic of dynamic fusion experimental design. Dynamic fusion links a single structural measure (i.e., GMV maps) to dynamic functional measures (i.e., windowed FNC matrices or subject average state connectomes) via multiple linked fusion experiments. Under the dynamic fusion framework, these can be performed as separate fusions to extract multiple functionally influenced structural basis sets. Post-hoc cross-fusion analysis is performed to assess the stability of both the structural and functional components derived across the linked fusions, as well as their temporal evolution over time.

Results

Cross-State Fusions Show Significant Functional Specification of Both Functional and Structural Component Maps at Rest

In both the HCP and the FBIRN datasets, we performed inter-state dynamic fusion (as well as intra-state fusion baselines) of GMV maps with different metrics of dFNC for each dataset (five FNC

states in HCP and six FBC states in FBIRN). Fig. 2 illustrates the cross-fusion stability of structural (left)

and functional (right) component maps for both FBIRN (top) and HCP (bottom) experiments. FBIRN

analyses included six intra-state pairs for baselines and 15 inter-state pairs for experimental results, and

HCP included ten intra-state pairs (five each for REST1 and REST2 scans) for baselines and 20 inter-state

pairs (ten each for REST1 and REST2 scans) for experimental results.

Across both datasets, intra-state baselines exhibit high stability across fusions in both structural and

functional components, providing the expected cross-fusion correspondence of component maps due to

random variation within a constant functional state or context. Experimental inter-state results showed

significantly lower cross-fusion correspondence/stability, or in other words, significant functional

specialization of component maps in both structural and functional fusion outputs. Given the structural

inputs to all cross-fusion comparisons was identical, paired with the significantly lowered cross-fusion

correlations compared to baselines, we can conclude that these component map variations, specifically

structural components, are driven by meaningful changes in functional patterns and thus meaningful

variations in state-specific structure-function coupling.

Overall, we observed relatively low inter-state correspondence for the functional components which was

expected as each of the functional inputs (dFNC states) have unique connectivity signatures, and, in the

case of the FBIRN experiments, are even found in distinct frequency bands. Though the GMV

components exhibited higher stability overall, we observed varying degrees of correspondence between

best-matched GMV components across independent fusion experiments, even though the structural inputs

were identical across each fusion. Specifically, we found fairly high cross-fusion correspondence ($|r| >$

0.5, shown in dotted lines in Fig. 2) in only the first few sorted component pairs, followed by a fairly

steep drop-off of component correspondence, indicating little overlap between a majority of the resultant

components. These consistent results across the two datasets suggest most of the structural components

identified via mCCA + jICA are significantly functionally influenced (i.e., "dynamic"), while a small

subset are less functionally influenced (i.e., "static"). This result further demonstrates the ability of

symmetric fusion approaches like mCCA + jICA to identify truly joint linkages in the data, as the changes

in the functional inputs resulted in considerably different structural outputs, despite accounting for a much

smaller portion of the entire dimensionality of the original input data. Moreover, our findings underscore

the importance of enabling flexible linkages between structure and changing function, as arbitrarily

imposing a limited structural basis would obfuscate the differential structure-function linkages that we

have identified via dynamic fusion.

Cross-Fusion Component Map Stability

Fig. 2. Cross-fusion stability of structural and functional component maps in both FBIRN (top) and HCP (bottom) dynamic fusion experiments. Static/dynamic threshold r = 0.50 shown in dotted line. Note that structural components are generally more stable across fusions (as expected), but interestingly a small subset of structural components are highly stable and another larger subset are more 'dynamic' that is they vary across fusions based on the context provided by the linked fMRI data.

Significant Schizophrenia/Control Group Differences were identified in both Static and Dynamic Components

For each of the 90 components derived across the six linked FBIRN state-level dynamic fusion experiments (model order = 15), we computed group differences between the structural component loading parameters (FDR corrected for multiple comparisons) and defined each component as "static" or "dynamic" (i.e., functionally uninfluenced or functionally influenced) based on the average cross-fusion

correlation > or < 0.5 across all pairs of cross-fusion experiments, respectively (Fig. 3). We found 9/17

static components exhibited significant group loading differences, as well as a majority (40/73) dynamic

components. We find the significance levels of many of the top dynamic components was directly on par

with those of the static components; in fact, the most significant group difference in structural loadings

was found in one of the most dynamic components (average cross-fusion correlation = 0.090). These

results further highlight the utility of functionally influenced dynamic structural components in capturing

clinically and diagnostically relevant features of structure-function coupling that are otherwise missed in

the static components. In Figures 4 and 5, we visualize the joint sources and highlight group effects for

some of the most significant components from both the dynamic and static sets.

Fig. 3. Significance of SZ/control group differences of GMV component loading parameters vs. average

cross-fusion correlation of best-matched component maps for each of the 90 components generated across

341   six state-level dynamic fusion experiments.

343 Joint sources for a pair of static components exhibiting significant group differences in loading

344 parameters are shown in Fig. 4. Static Joint Source 1 was derived from fusion with functional data from a

345 low-frequency state (State 1 in (Duda et al., 2022)), and exhibited an average cross-fusion correlation of

0.618 as well as group differences in GMV component loading parameters at a significance level p = 9.14e-07. Static Joint Source 2 was derived from fusion with functional data from a mid-frequency state (State 5 in (Duda et al., 2022)), and exhibited an average cross-fusion correlation of 0.598 as well as group differences in GMV component loading parameters at a significance level p = 4.08e-08. Though both derived from fusions with notably different functional contexts, as underscored by the lack of overlap in most edges in the functional components for each joint source, the structural component maps are highly similar across the fusions (r = 0.738), with peaks in cingulate and orbitofrontal regions. These paired sources illustrate structural components that are not strongly influenced by their link to function, which can be understood as "static" or "global" structural components. This is also reflected in the joint histograms depicting loading parameter group differences – across both joint sources the SZ and CON groups are more readily separable across the structural loading axis and more overlapped across the functional loadings axis, suggesting an overall weaker influence of the functional inputs compared to the structural inputs to the entire joint source.

Fig. 4. Joint sources of paired static components with significant group differences in loading parameters.
Static Joint Source 1 was derived from dynamic fusion to a low-frequency state (State 1), while Static
Joint Source 2 was derived from dynamic fusion to a mid-frequency state (State 6). Structural component
maps are highly similar, both exhibiting peaks in cingulate and orbitofrontal regions, while linked
functional components show little overlap. See (Duda et al., 2022) for more details on FBC states.
Abbreviations: subcortical (SC), auditory (AUD), sensorimotor (SM), visual (VIS), cognitive control
(CC), default mode (DM), cerebellum (CB), schizophrenia (SZ), control (CON).
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We highlight two dynamic joint sources in Fig. 5. Dynamic Joint Source 1 was derived from a CON-
dominant mid-frequency state (State 4 in (Duda et al., 2022)) and Dynamic Joint Source 2 was derived
from dynamic fusion to an SZ-dominant high-frequency state (State 6 in (Duda et al., 2022)). Dynamic
Joint Source 1 exhibits peaks across the anterior cingulate cortex, insula, and superior parietal regions, has
an average cross-fusion correlation of 0.0.90 and group differences in structural component loading
params at the significance level p = 3.82-08, making it among one of the most dynamic (i.e., most
functionally influenced/functionally specialized) components, as well as the component with the most
significant group differences in structural loading parameters. Dynamic Joint Source 2 exhibits peaks in
cognitive control regions, including the insula and inferior parietal lobule, has an average cross-fusion
correlation of 0.299 and exhibited strong group differences in structural component loading params at the
significance level p = 1.73e-07. As expected, the functional components for each dynamic joint source are
unique, but some interesting similarities do appear – for example the fusiform gyrus (FFG) within the
visual domain as well as CB2 in the cerebellum serve as functional hubs in both functional components.
Dynamic Joint Source 1 is marked by positive connections between VIS and CB, SC, and CC regions, as
well as CB-SM, and both FFG-DM and SC-CC anticorrelations. Dynamic Joint Source 2 is marked by
negative edges connecting SM-DM regions, as well as between FFG and SC, CB and CC regions, and
positive correlations between CB and DM, CC and SC regions, particularly caudate and thalamus. Further
examination of the dual histograms of loading parameter group differences, we observe tighter
concentration of SZ and CON subjects within both the structural and functional loading parameter spaces
than was observed for the static sources, as well as more distinct separability of the groups in both the
structural and functional parameter axes, suggesting a stronger contribution of both inputs into the joint
solution.

Fig. 5. Joint sources of two exemplar dynamic components with significant group differences in loading parameters. Dynamic Joint Source 1 was derived from dynamic fusion to a CON-dominant mid-frequency state (State 4) and Dynamic Joint Source 2 was derived from dynamic fusion to an SZ-dominant high-frequency state (State 6). The structural map for Dynamic Joint Source 1 shows peaks in the cingulate cortex and superior parietal lobule, while the structural map for Dynamic Joint Source 2 shows peaks in inferior parietal cognitive control regions as well as the insula. Joint loading histograms show tight concentration of both SZ and CON subjects, and strong separations on both the structural and functional component axes, indicating strong contributions of both the structural and functional data to the joint sources. See (Duda et al., 2022) for more details on FBC states. Abbreviations: subcortical (SC), auditory (AUD), sensorimotor (SM), visual (VIS), cognitive control (CC), default mode (DM), cerebellum (CB), schizophrenia (SZ), control (CON).

Organization of Static/Dynamic Structure/Function Coupling in Healthy Brains Aligns to

Unimodal/Transmodal Hierarchical Segregation of Cortex

After establishing both the cognitive relevance (Fig 2) and clinical utility (Figs 3-5) of joint sources

derived via dynamic fusion, we interrogated the organization of strongly static or strongly dynamic

regions in the brain. Thus, we applied our dynamic fusion pipeline in both HCP REST1_LR and

REST2_LR fMRI time series (henceforth termed Rest1 and Rest2), collected with the same scan

parameters on the same subjects on both their initial and return study visits (Van Essen et al., 2013). In

both experiments, 5 dFNC states were derived via k-means and model order = 15 were used for fusion,

resulting in 75 joint sources each for both Rest1 and Rest2. As was done in the FBIRN analysis, greedy

cross-fusion matching and correlation of structural component maps was performed separately in both

experiments, and components were ranked and labeled as "dynamic" or "static" according to their

stability score (i.e., average cross-fusion correlations) < or > 0.5, respectively. After filtering of spurious

components, we selected the top 10 most static (i.e., highest stability scores) and top 10 most dynamic

(i.e., lowest stability scores) components. For each set of static/dynamic components, component maps

are aggregated as follows: first, component maps are thresholded for significance ($|z| >= 2$), then $|z|$ maps

are normalized to [0, 1], weighted by stability score (or 1-stability score in the case of dynamic

components), and aggregated by taking the max value at each voxel. For both experiments, we subtract

the dynamic map from the static map to obtain composite differential stability maps across the whole

brain, and finally average the Rest1 and Rest2 maps to obtain a global view of brain organization into

statically/dynamically linked regions (Fig. 6).

From the structural differential stability map, we can observe the organization of the brain into clear hubs

of static and dynamic structure/function linkage, as well as mixed regions that exhibit both properties.

Static hubs are comprised mostly of regions in the anterior cingulate and visual regions, whereas dynamic

hubs are found in the insula, default mode regions and subcortical structures. These patterns are also

reflected in the differential functional component map – the insula, inferior parietal lobule, posterior

cingulate, precuneus and subcortical structures including putamen and caudate are all marked by stronger

edges in dynamic components, whereas visual, sensorimotor and anterior cingulate regions all serve as

hubs for edges in predominantly static joint sources. We note that our results align well to the widely-

studied unimodal-transmodal principal functional gradient (Margulies et al., 2016), where we find static

hubs align to the extremes of the unimodal (i.e., visual cortex) – transmodal (i.e., association

cortex/anterior cingulate regions) cortical structures, whereas dynamic hubs are comprised of

intermediary regions along this gradient (i.e., insular cortex). This organization of time-varying structure-function coupling throughout the brain quite closely mirrors recent work published in (Liu et al., 2022).

Fig. 6. Average of Rest1 and Rest2 differential stability maps in both structural and functional components. Structural maps reveal organization of the brain into regions hallmarked by static (anterior cingulate, visual regions) and dynamic (default mode, subcortical regions, insula) structure/function linkages. This segregation aligns well to unimodal/transmodal hierarchical lines.

White Matter Components Also Show Strong Links to Temporally Evolving FNC

Of the total 833 HCP subjects, 737 had processed FA maps available, thus we replicated the state-level HCP dynamic fusion experiments in this subset of subjects using white matter FA maps as the structural inputs with model order = 10. Results comparing the GMV and FA dynamic fusion experiments with the same model order are shown in Fig. 7. While the overarching relationship between structure and function holds in the FA data (higher stability in structural components than functional components), there are a few key differences to highlight. First, the FA experiment shows evidence for just one highly static (mean cross-fusion correlation = 0.75), with a steep drop-off to the rest as dynamic components, as opposed to a gradual decrease in cross-fusion stability and two or three "static" component maps. Second, the overall cross-fusion stability of the components is lower in the FA experiments compared to GMV. This result

may suggest a stronger linkage to the changing functional manifolds in each distinct dFNC state fusion,

thus leading to lowered cross-fusion stability. To assess this hypothesis, we compared the correlations

between the structural and functional loading parameters for all components in the GMV and FA

experiments and found that the correlations were indeed higher in the FNC + FA components (p = 0.0043,

t = -2.927). These results may suggest that white matter FA components can be more susceptible to

influence of changing functional inputs than GMV maps in symmetric data fusion approaches like mCCA

+ jICA.

Fig. 7. White matter (FA) components show one highly stable component, with a steep drop-off to

dynamic components that show overall lower cross-fusion stability than corresponding GMV components

in the same subjects (top panels). Higher correlation between structural and functional loading parameters

was observed in FA fusion experiments compared to GMV fusion (bottom panel; p = 0.0043, t = -2.927).

Discussion

Here, we propose an approach for identifying flexible, dynamic linkages between brain structure

and time-varying brain function, termed dynamic fusion. Though previous studies have examined time-

resolved coupling of brain structure and function (Duda et al., 2022; Iraji et al., 2019; Liu et al., 2022; Plis

et al., 2018), to the best of our knowledge our work is the first to jointly estimate voxel-wise structural

components as a function of time, and thus as a function of structure's changing linkage to dynamic brain

function. Our approach is fully data driven and allows both modalities (or all when 3+ modalities are

used) to contribute to the fusion equally (i.e., symmetric fusion), thus enforcing fewer assumptions and

enabling a broader spectrum of flexibility than recent symmetric and asymmetric fusion works in

structural dynamics. The findings outlined in this paper emphasize how conducting multiple linked

fusions can greatly increase the versatility and interpretability of multimodal analyses.

We show that dynamic fusion identifies functionally adaptive neuroanatomical basis sets related

to changing functional manifolds at the dFNC state-level. To fully appreciate these results, we wish to

underscore that the structural inputs are identical at each independent fusion within a given experiment,

thus *any change in the resultant structural component maps is driven solely by its varying linkage to the*

changing functional inputs at each window/state. When applied in resting state data, we find only a few

GMV components are consistently derived with high correspondence when jointly estimated with

changing functional manifolds (Fig. 2), while the vast majority show evidence of more significant

functional influences. These results held across numerous experiments encompassing different data sets

(HCP vs. FBIRN), subject cohorts (CON vs. SZ), dynamic FNC approaches (SWPC vs. FBC), and even

structural inputs (GMV vs. FA maps). Taken together, these results exemplify mCCA + jICA's capacity to

identify truly joint linkages in the data to produce structural components that are indeed functionally

influenced. Moreover, our findings underscore the importance of enabling flexible linkages between

structure and function, especially as a function of the dynamic brain changes over time. Without the

natural flexibility afforded by the mCCA + jICA algorithm, as well as the flexibility imparted by

conducting multiple linked fusions as the novelty of the approach taken in this work, the nuanced joint

structure-function relationships would have remained hidden in the data (Sui et al., 2013).

In addition to the cross-fusion stability of components related to changing cognitive demands, we

found that a large portion (40/73) of dynamic components showed significant group differences between

SZ and controls in the FBIRN resting state experiments, with the most significant group difference

belonging to a highly dynamic component (Fig. 5). Based on this result, we can conclude functionally

influenced structural components can indeed capture the changes in the relationship between structure and

dynamic brain function of clinical and diagnostic relevance. By assessing the full structural/functional

loading parameter space we also conclude that dynamic components show stronger separability along

both structural and functional loading parameter axes than comparable static components, suggesting

dynamic components do, indeed, represent a more harmonious joint influence of structure and function on

the joint source overall and thus better capture the complex interplay of structure and function

underpinning both clinical and control populations.

Moreover, by applying dynamic fusion in a set of healthy control data from the HCP cohort we

generated a map of global differential stability, organizing the brain into regions of static and dynamic

functional linkages. We found static hubs aligned to the extremes of the unimodal (i.e., visual cortex) –

transmodal (i.e., association cortex/anterior cingulate regions) hierarchy of cortical structures, whereas

dynamic hubs were comprised of intermediary regions along this gradient (i.e., insular cortex) (Margulies

et al., 2016). The significance of this result is two-fold: 1) it upholds and closely mirrors results of a

recently published study which utilized multilinear regression to evaluate time-resolved structure-function

coupling in atlas-derived brain networks (Liu et al., 2022), and 2) further underscores the neurobiological

relevance of sources derived via our dynamic fusion approach.

It is thought that the unimodal-transmodal gradient reflects a similar gradient in connection

lengths across the cortex (Oligschläger et al., 2019; Sepulcre et al., 2010). Thus, it is possible that the

stability observed at the poles of this gradient are also a reflection of connection lengths – speculatively,

this could stem from the ease of maintaining shorter connections and the importance of stabilizing critical

long-range connections. In their work, (Liu et al., 2022) found this same U-shaped relationship between

stability and connection length, with highest stability at the shortest and longest extremes and increased

dynamicity for those networks with mid-range connection length. Our results corroborate this finding and

warrant future exploration into connection lengths as a facet of structure-function dynamics.

One of the clearest dynamically linked structure-function hubs in both our study and (Liu et al.,

2022) is the insula. The insula is a key region in the ventral attention/salience network that dynamically

fields and coordinates communication of both unimodal (e.g., sensory) and transmodal (e.g., frontal)

regions (Ghaziri et al., 2017; Tian & Zalesky, 2018). Taken together with our results, we echo the

speculations presented in (Liu et al., 2022) and suggest that dynamic structure-function coupling

exhibited within the insular cortex could reflect flexible integration and transmission of various neural

signals though this complex cortical hub. Thus, states that result in dynamic structural components with

peaks in insula could be thought of as "salience" states in which attention is being directed or integrated

within the cortex.

This work represents a reduced-case feasibility study of a wider dynamic fusion framework (Fig

1). Our results clearly demonstrate the utility of estimating flexible linkages between structure and

dynamic brain function, and thus motivate the extension of dynamic fusion to a more advanced model. In

our next step, we plan to extend this work into a unified fusion framework that will jointly estimate

multiple structural basis sets at once based on unique linkages between structural and temporally evolving

functional inputs. In addition to the flexibility of coupling between neuroanatomical measures and

dynamic connections between functional networks, we may also consider incorporating flexibility in the

structural definitions of the functional networks themselves. Future work could employ dynamic spatially

constrained ICA (Duda et al., 2023; Iraji et al., 2019) to extract individualized time-varying functional
entities with flexible spatial maps at each window in the dynamic analysis. Such an analysis could be
done using the original 53 ICNs defines in the Neuromark_1.0 template, or be expanded to the multiscale
Neuromark template (http://trendscenter.org/data), which defines 105 ICNs derived across multiple spatial
and temporal scales (Iraji et al., 2023), further increasing the precision with which we can investigate
dynamic structural and functional coupling in a data-driven manner.

Other future directions may involve extending the analyses described here by applying 3-way
dynamic fusion to enable deeper investigation into the connection of both gray matter and white matter
structure to temporally evolving brain function, as well as how hidden linkages between the structural
modalities affect the joint estimation of the structural components. Interestingly, one result in our study
suggested that white matter FA components were potentially more susceptible to functional influence in
the joint fusion than GMV components in the same subjects (Fig. 7). Future work will be needed to
replicate these results and further investigate the nature of white matter structure/gray matter function
linkages. A newly developed ICA-based approach has enabled joint estimation of linked structural and
functional connectivity from dMRI and fMRI data (Wu et al., 2015; Wu & Calhoun, 2023). Future work
could leverage this approach under the dynamic fusion framework further address time varying structure-
function linkages between white matter and FNC. Thus far, the analysis of brain function is largely
focused on grey matter regions, leaving functional activity and connectivity within white matter regions
relatively understudied. In fact, in data-driven analyses, functional components whose structural maps
reside largely within white matter are often discarded as noise components. Exploration of the role of
these white matter functional components in the context of whole brain function and cognition is
currently underway. Future work including white matter functional components would further
contextualize the investigation into dynamic structure-function coupling with tissue-level specificity on
both ends.

In conclusion, we present an approach for dynamic fusion of multimodal neuroimaging data as a
method for studying time-varying structure-function coupling. Components derived from our dynamic
fusion approach exhibit strong cognitive, clinical and neurobiological correlates, underscoring the
importance of retaining rich temporal dynamic information in studies of structure-function linkage.
Overall, our results support the claim that patterns of structure-function coupling are both regionally
heterogenous and temporally varying and provide an important next step in developing a model of
dynamical linkage between brain function and structure.

Data and Code Availability

Details for the availability of the FBIRN dataset used in this paper can be found here:

https://www.nitrc.org/projects/fbirn/.

Details for the availability of the HCP dataset used in this paper can be found here:

https://www.humanconnectome.org/study/hcp-young-adult.

Code and documentation for running mCCA + jICA fusion can be found in the FIT toolbox here:

https://trendscenter.org/software/.

Author Contributions

This study was conceived and designed by MD & VDC. Coding, analysis, visualization of results, and

initial drafting of manuscript was performed by MD. All authors participated in interpretation of results

and editing the final manuscript.

Declaration of Competing Interests

The authors declare no competing interests.

References

Abrol, A., Rashid, B., Rachakonda, S., Damaraju, E., & Calhoun, V. D. (2017). Schizophrenia Shows
Disrupted Links between Brain Volume and Dynamic Functional Connectivity. *Frontiers in Neuroscience*, *11*. https://www.frontiersin.org/articles/10.3389/fnins.2017.00624

Allen, E. A., Damaraju, E., Plis, S. M., Erhardt, E. B., Eichele, T., & Calhoun, V. D. (2014). Tracking
whole-brain connectivity dynamics in the resting state. *Cerebral Cortex (New York, N.Y.: 1991)*, *24*(3), 663–676. https://doi.org/10.1093/cercor/bhs352

Andersson, J. L. R., Skare, S., & Ashburner, J. (2003). How to correct susceptibility distortions in spin-
echo echo-planar images: Application to diffusion tensor imaging. *NeuroImage*, *20*(2), 870–888. https://doi.org/10.1016/S1053-8119(03)00336-7

Andersson, J. L. R., & Sotiropoulos, S. N. (2016). An integrated approach to correction for off-resonance
effects and subject movement in diffusion MR imaging. *NeuroImage*, *125*, 1063–1078. https://doi.org/10.1016/j.neuroimage.2015.10.019

Avants, B. B., Tustison, N., & Johnson, H. (2009). Advanced Normalization Tools (ANTS). *Insight J*, *2*(365), 1–35.

Battaglia, D., Boudou, T., Hansen, E. C. A., Lombardo, D., Chettouf, S., Daffertshofer, A., McIntosh, A.
R., Zimmermann, J., Ritter, P., & Jirsa, V. (2020). Dynamic Functional Connectivity between order and randomness and its evolution across the human adult lifespan. *NeuroImage*, *222*, 117156. https://doi.org/10.1016/j.neuroimage.2020.117156

Baum, G. L., Cui, Z., Roalf, D. R., Ciric, R., Betzel, R. F., Larsen, B., Cieslak, M., Cook, P. A., Xia, C.
H., Moore, T. M., Ruparel, K., Oathes, D. J., Alexander-Bloch, A. F., Shinohara, R. T., Raznahan, A., Gur, R. E., Gur, R. C., Bassett, D. S., & Satterthwaite, T. D. (2020). Development of structure–function coupling in human brain networks during youth. *Proceedings of the National Academy of Sciences*, *117*(1), 771–778. https://doi.org/10.1073/pnas.1912034117

Calhoun, V. D., Miller, R., Pearlson, G., & Adalı, T. (2014). The Chronnectome: Time-Varying

Connectivity Networks as the Next Frontier in fMRI Data Discovery. *Neuron*, *84*(2), 262–274.

https://doi.org/10.1016/j.neuron.2014.10.015

Calhoun, V. D., & Sui, J. (2016). Multimodal Fusion of Brain Imaging Data: A Key to Finding the

Missing Link(s) in Complex Mental Illness. *Biological Psychiatry: Cognitive Neuroscience and*

Neuroimaging, *1*(3), 230–244. https://doi.org/10.1016/j.bpsc.2015.12.005

Calhoun, V., Wu, L., Kiehl, K., Eichele, T., & Pearlson, G. (2010). Aberrant Processing of Deviant

Stimuli in Schizophrenia Revealed by Fusion of FMRI and EEG Data. *Acta Neuropsychiatrica*,

22(3), 127–138. https://doi.org/10.1111/j.1601-5215.2010.00467.x

Chang, C., & Glover, G. H. (2010). Time–frequency dynamics of resting-state brain connectivity

measured with fMRI. *NeuroImage*, *50*(1), 81–98.

https://doi.org/10.1016/j.neuroimage.2009.12.011

Damaraju, E., Allen, E. A., Belger, A., Ford, J. M., McEwen, S., Mathalon, D. H., Mueller, B. A.,

Pearlson, G. D., Potkin, S. G., Preda, A., Turner, J. A., Vaidya, J. G., van Erp, T. G., & Calhoun,

V. D. (2014). Dynamic functional connectivity analysis reveals transient states of dysconnectivity

in schizophrenia. *NeuroImage. Clinical*, *5*, 298–308. https://doi.org/10.1016/j.nicl.2014.07.003

DeRamus, T. P., Wu, L., Qi, S., Iraji, A., Silva, R., Du, Y., Pearlson, G., Mayer, A., Bustillo, J. R.,

Stromberg, S. F., & Calhoun, V. D. (2022). Multimodal data fusion of cortical-subcortical

morphology and functional network connectivity in psychotic spectrum disorder. *NeuroImage.*

Clinical, *35*, 103056. https://doi.org/10.1016/j.nicl.2022.103056

Du, Y., Fu, Z., Sui, J., Gao, S., Xing, Y., Lin, D., Salman, M., Abrol, A., Rahaman, M. A., Chen, J., Hong,

L. E., Kochunov, P., Osuch, E. A., Calhoun, V. D., & Alzheimer's Disease Neuroimaging

Initiative. (2020). NeuroMark: An automated and adaptive ICA based pipeline to identify

reproducible fMRI markers of brain disorders. *NeuroImage. Clinical*, *28*, 102375.

https://doi.org/10.1016/j.nicl.2020.102375

Duda, M., Faghiri, A., & Calhoun, V. D. (2022). Multimodal Analysis Uncovers Links between Grey Matter Volume and both Low-and High-frequency Dynamic Connectivity States in Schizophrenia. *2022 IEEE International Conference on Bioinformatics and Biomedicine (BIBM)*, 1521–1525. https://doi.org/10.1109/BIBM55620.2022.9995415

Duda, M., Iraji, A., Ford, J. M., Lim, K. O., Mathalon, D. H., Mueller, B. A., Potkin, S. G., Preda, A., Van Erp, T. G. M., & Calhoun, V. D. (2023). Reliability and clinical utility of spatially constrained estimates of intrinsic functional networks from very short fMRI scans. *Human Brain Mapping*, *44*(6), 2620–2635. https://doi.org/10.1002/hbm.26234

Faghiri, A., Iraji, A., Damaraju, E., Turner, J., & Calhoun, V. D. (2021). A unified approach for characterizing static/dynamic connectivity frequency profiles using filter banks. *Network Neuroscience*, *5*(1), 56–82. https://doi.org/10.1162/netn_a_00155

Fukushima, M., Betzel, R. F., He, Y., van den Heuvel, M. P., Zuo, X.-N., & Sporns, O. (2018). Structure-function relationships during segregated and integrated network states of human brain functional connectivity. *Brain Structure & Function*, *223*(3), 1091–1106. https://doi.org/10.1007/s00429-017-1539-3

Fukushima, M., & Sporns, O. (2020). Structural determinants of dynamic fluctuations between segregation and integration on the human connectome. *Communications Biology*, *3*(1), Article 1. https://doi.org/10.1038/s42003-020-01331-3

Geenjaar, E. P. T., Lewis, N. L., Fedorov, A., Wu, L., Ford, J. M., Preda, A., Plis, S. M., & Calhoun, V. D. (2023). Chromatic fusion: Generative multimodal neuroimaging data fusion provides multi-informed insights into schizophrenia. *medRxiv*, 2023.05.18.23290184. https://doi.org/10.1101/2023.05.18.23290184

Ghaziri, J., Tucholka, A., Girard, G., Houde, J.-C., Boucher, O., Gilbert, G., Descoteaux, M., Lippé, S., Rainville, P., & Nguyen, D. K. (2017). The Corticocortical Structural Connectivity of the Human Insula. *Cerebral Cortex*, *27*(2), 1216–1228. https://doi.org/10.1093/cercor/bhv308

Glasser, M. F., Coalson, T. S., Robinson, E. C., Hacker, C. D., Harwell, J., Yacoub, E., Ugurbil, K.,

Andersson, J., Beckmann, C. F., Jenkinson, M., Smith, S. M., & Van Essen, D. C. (2016). A

multi-modal parcellation of human cerebral cortex. *Nature*, *536*(7615), Article 7615.

https://doi.org/10.1038/nature18933

Griffa, A., Amico, E., Liégeois, R., Van De Ville, D., & Preti, M. G. (2022). Brain structure-function

coupling provides signatures for task decoding and individual fingerprinting. *NeuroImage*, *250*,

118970. https://doi.org/10.1016/j.neuroimage.2022.118970

Iraji, A., Deramus, T. P., Lewis, N., Yaesoubi, M., Stephen, J. M., Erhardt, E., Belger, A., Ford, J. M.,

McEwen, S., Mathalon, D. H., Mueller, B. A., Pearlson, G. D., Potkin, S. G., Preda, A., Turner, J.

A., Vaidya, J. G., van Erp, T. G. M., & Calhoun, V. D. (2019). The spatial chronnectome reveals a

dynamic interplay between functional segregation and integration. *Human Brain Mapping*,

40(10), 3058–3077. https://doi.org/10.1002/hbm.24580

Iraji, A., Faghiri, A., Lewis, N., Fu, Z., Rachakonda, S., & Calhoun, V. D. (2021). Tools of the trade:

Estimating time-varying connectivity patterns from fMRI data. *Social Cognitive and Affective*

Neuroscience, *16*(8), 849–874. https://doi.org/10.1093/scan/nsaa114

Iraji, A., Fu, Z., Faghiri, A., Duda, M., Chen, J., Rachakonda, S., DeRamus, T., Kochunov, P., Adhikari, B.

M., Belger, A., Ford, J. M., Mathalon, D. H., Pearlson, G. D., Potkin, S. G., Preda, A., Turner, J.

A., van Erp, T. G. M., Bustillo, J. R., Yang, K., … Calhoun, V. D. (2023). Identifying canonical

and replicable multi-scale intrinsic connectivity networks in 100k+ resting-state fMRI datasets.

Human Brain Mapping, *44*(17), 5729–5748. https://doi.org/10.1002/hbm.26472

Keator, D. B., van Erp, T. G. M., Turner, J. A., Glover, G. H., Mueller, B. A., Liu, T. T., Voyvodic, J. T.,

Rasmussen, J., Calhoun, V. D., Lee, H. J., Toga, A. W., McEwen, S., Ford, J. M., Mathalon, D. H.,

Diaz, M., O'Leary, D. S., Jeremy Bockholt, H., Gadde, S., Preda, A., … FBIRN. (2016). The

Function Biomedical Informatics Research Network Data Repository. *NeuroImage*, *124*(Pt B),

1074–1079. https://doi.org/10.1016/j.neuroimage.2015.09.003

698 Khalilullah, K. M. I., Agcaoglu, O., Sui, J., Adali, T., Duda, M., & Calhoun, V. D. (2023). Multimodal

699   fusion of multiple rest fMRI networks and MRI gray matter via multilink joint ICA reveals highly

700   significant function/structure coupling in Alzheimer's disease. *bioRxiv: The Preprint Server for*

701   *Biology*, 2023.02.28.530458. https://doi.org/10.1101/2023.02.28.530458

702 Liu, Z.-Q., Vázquez-Rodríguez, B., Spreng, R. N., Bernhardt, B. C., Betzel, R. F., & Misic, B. (2022).

703   Time-resolved structure-function coupling in brain networks. *Communications Biology*, *5*(1),

704   Article 1. https://doi.org/10.1038/s42003-022-03466-x

705 Lottman, K. K., White, D. M., Kraguljac, N. V., Reid, M. A., Calhoun, V. D., Catao, F., & Lahti, A. C.

706   (2018). Four-way multimodal fusion of 7 T imaging data using an mCCA+jICA model in first-

707   episode schizophrenia. *Human Brain Mapping*, *39*(4), 1475–1488.

708   https://doi.org/10.1002/hbm.23906

709 Lurie, D. J., Kessler, D., Bassett, D. S., Betzel, R. F., Breakspear, M., Kheilholz, S., Kucyi, A., Liégeois,

710   R., Lindquist, M. A., McIntosh, A. R., Poldrack, R. A., Shine, J. M., Thompson, W. H., Bielczyk,

711   N. Z., Douw, L., Kraft, D., Miller, R. L., Muthuraman, M., Pasquini, L., … Calhoun, V. D.

712   (2020). Questions and controversies in the study of time-varying functional connectivity in

713   resting fMRI. *Network Neuroscience*, *4*(1), 30–69. https://doi.org/10.1162/netn_a_00116

714 Margulies, D. S., Ghosh, S. S., Goulas, A., Falkiewicz, M., Huntenburg, J. M., Langs, G., Bezgin, G.,

715   Eickhoff, S. B., Castellanos, F. X., Petrides, M., Jefferies, E., & Smallwood, J. (2016). Situating

716   the default-mode network along a principal gradient of macroscale cortical organization.

717   *Proceedings of the National Academy of Sciences*, *113*(44), 12574–12579.

718   https://doi.org/10.1073/pnas.1608282113

719 Oligschläger, S., Xu, T., Baczkowski, B. M., Falkiewicz, M., Falchier, A., Linn, G., & Margulies, D. S.

720   (2019). Gradients of connectivity distance in the cerebral cortex of the macaque monkey. *Brain*

721   *Structure and Function*, *224*(2), 925–935. https://doi.org/10.1007/s00429-018-1811-1

Pang, J. C., Aquino, K. M., Oldehinkel, M., Robinson, P. A., Fulcher, B. D., Breakspear, M., & Fornito, A.

(2023). Geometric constraints on human brain function. *Nature*, *618*(7965), Article 7965.

https://doi.org/10.1038/s41586-023-06098-1

Plis, S. M., Amin, M. F., Chekroud, A., Hjelm, D., Damaraju, E., Lee, H. J., Bustillo, J. R., Cho, K.,

Pearlson, G. D., & Calhoun, V. D. (2018). Reading the (functional) writing on the (structural)

wall: Multimodal fusion of brain structure and function via a deep neural network based

translation approach reveals novel impairments in schizophrenia. *NeuroImage*, *181*, 734–747.

https://doi.org/10.1016/j.neuroimage.2018.07.047

Preti, M. G., Bolton, T. A., & Van De Ville, D. (2017). The dynamic functional connectome: State-of-the-

art and perspectives. *NeuroImage*, *160*, 41–54. https://doi.org/10.1016/j.neuroimage.2016.12.061

Preti, M. G., & Van De Ville, D. (2019). Decoupling of brain function from structure reveals regional

behavioral specialization in humans. *Nature Communications*, *10*(1), Article 1.

https://doi.org/10.1038/s41467-019-12765-7

Qi, S., Silva, R. F., Zhang, D., Plis, S. M., Miller, R., Vergara, V. M., Jiang, R., Zhi, D., Sui, J., &

Calhoun, V. D. (2022). Three-way parallel group independent component analysis: Fusion of

spatial and spatiotemporal magnetic resonance imaging data. *Human Brain Mapping*, *43*(4),

1280–1294. https://doi.org/10.1002/hbm.25720

Sepulcre, J., Liu, H., Talukdar, T., Martincorena, I., Yeo, B. T. T., & Buckner, R. L. (2010). The

Organization of Local and Distant Functional Connectivity in the Human Brain. *PLOS*

Computational Biology, *6*(6), e1000808. https://doi.org/10.1371/journal.pcbi.1000808

Sui, J., Adali, T., Yu, Q., Chen, J., & Calhoun, V. D. (2012). A review of multivariate methods for

multimodal fusion of brain imaging data. *Journal of Neuroscience Methods*, *204*(1), 68–81.

https://doi.org/10.1016/j.jneumeth.2011.10.031

Sui, J., He, H., Pearlson, G. D., Adali, T., Kiehl, K. A., Yu, Q., Clark, V. P., Castro, E., White, T., Mueller,

B. A., Ho, B. C., Andreasen, N. C., & Calhoun, V. D. (2013). Three-way (N-way) fusion of brain

imaging data based on mCCA+jICA and its application to discriminating schizophrenia. *NeuroImage*, *66*, 119–132. https://doi.org/10.1016/j.neuroimage.2012.10.051

Sui, J., Pearlson, G., Caprihan, A., Adali, T., Kiehl, K. A., Liu, J., Yamamoto, J., & Calhoun, V. D. (2011). Discriminating schizophrenia and bipolar disorder by fusing fMRI and DTI in a multimodal CCA+ joint ICA model. *NeuroImage*, *57*(3), 839–855. https://doi.org/10.1016/j.neuroimage.2011.05.055

Tian, Y., & Zalesky, A. (2018). Characterizing the functional connectivity diversity of the insula cortex: Subregions, diversity curves and behavior. *NeuroImage*, *183*, 716–733. https://doi.org/10.1016/j.neuroimage.2018.08.055

Van Essen, D. C., Smith, S. M., Barch, D. M., Behrens, T. E. J., Yacoub, E., & Ugurbil, K. (2013). The WU-Minn Human Connectome Project: An overview. *NeuroImage*, *80*, 62–79. https://doi.org/10.1016/j.neuroimage.2013.05.041

Vázquez-Rodríguez, B., Suárez, L. E., Markello, R. D., Shafiei, G., Paquola, C., Hagmann, P., van den Heuvel, M. P., Bernhardt, B. C., Spreng, R. N., & Misic, B. (2019). Gradients of structure-function tethering across neocortex. *Proceedings of the National Academy of Sciences of the United States of America*, *116*(42), 21219–21227. https://doi.org/10.1073/pnas.1903403116

Vergara, V. M., Ulloa, A., Calhoun, V. D., Boutte, D., Chen, J., & Liu, J. (2014). A three-way parallel ICA approach to analyze links among genetics, brain structure and brain function. *NeuroImage*, *98*, 386–394. https://doi.org/10.1016/j.neuroimage.2014.04.060

Wu, L., & Calhoun, V. (2023). Joint connectivity matrix independent component analysis: Auto-linking of structural and functional connectivities. *Human Brain Mapping*, *44*(4), 1533–1547. https://doi.org/10.1002/hbm.26155

Wu, L., Calhoun, V. D., Jung, R. E., & Caprihan, A. (2015). Connectivity-based whole brain dual parcellation by group ICA reveals tract structures and decreased connectivity in schizophrenia. *Human Brain Mapping*, *36*(11), 4681–4701. https://doi.org/10.1002/hbm.22945