1   Proactive, Reactive, and Attentional Dynamics: An Integrative Model of Cognitive Control
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Abstract

We developed a novel Proactive Reactive and Attentional Dynamics (PRAD) computational

model designed to dissect the latent mechanisms of inhibitory control in human cognition.

Leveraging data from over 7,500 participants in the NIH Adolescent Brain Cognitive

Development study, we demonstrate that PRAD surpasses traditional models by integrating

proactive, reactive, and attentional components of inhibitory control. Employing a hierarchical

Bayesian framework, PRAD offers a granular view of the dynamics underpinning action

execution and inhibition, provides debiased estimates of stop-signal reaction times, and

elucidates individual and temporal variability in cognitive control processes. Our findings reveal

significant intra-individual variability, challenging conventional assumptions of random

variability across trials. By addressing nonergodicity and systematically accounting for the multi-

componential nature of cognitive control, PRAD advances our understanding of the cognitive

mechanisms driving individual differences in cognitive control and provides a sophisticated

computational framework for dissecting dynamic cognitive processes across diverse populations.

Our integrative approach significantly advances psychological theory about the multiple

neurocognitive processes underlying cognitive control. We also demonstrate the relevance of our

theoretical and modeling framework to understand the cognitive, neural, clinical, and exposomic

factors related to cognitive control.

Human cognition is a dynamic process, which relies in part, on goal-directed beliefs about task

characteristics, context-dependent flexible action control, the capacity to learn from a history of

decisions and consequences, leading to moment-to-moment adaptation of response strategies to

optimize behavioral outcomes (A. R. Aron, 2011; T. S. Braver, 2012; Todd S Braver, Paxton,

Locke, & Barch, 2009; Cai et al., 2016; Menon, Adleman, White, Glover, & Reiss, 2001).

Impairments in cognitive systems that regulate such dynamic processes underlying everyday

cognitive functioning are a hallmark of psychopathology (Casey, Tottenham, Liston, & Durston,

2005; Menon, 2011, 2013; Nigg, 2017; Toga, Thompson, & Sowell, 2006). Identifying latent

cognitive factors that drive adaptive and maladaptive behavioral dynamics is critical for

understanding individual differences in how cognitive processes unfold over time, and how their

associated alterations in regulatory systems affect symptom presentation in neuropsychiatric

disorders (Hall, Bernat, & Patrick, 2007; Ivanov, Schulz, London, & Newcorn, 2008;

Korenblum, Chen, Manassis, & Schachar, 2007; Murray & Kochanska, 2002; Olvet & Hajcak,

2008; Oosterlaan & Sergeant, 1996; R. Schachar, Tannock, Marriott, & Logan, 1995; R. J.

Schachar et al., 2004). However, conventional methods are often unable to reveal multi-

componential latent constructs that govern dynamic cognitive control processes.

Here, we develop Proactive Reactive and Attentional Dynamics (PRAD), a novel computational

model to characterize and measure latent cognitive constructs that govern behavioral dynamics

of action execution and inhibition, whose deficits are often associated with multiple psychiatric

disorders including attention deficit hyperactivity disorder, autism, substance abuse, and

schizophrenia. This model was applied to a response inhibition paradigm in the large-scale (N >

7500) Adolescent Brain Cognitive Development (ABCD) (B. Casey et al., 2018) study to

uncover the mechanisms by which dynamic cognitive processes involved in response initiation

and inhibition are regulated, and the nature of individual differences in the latent cognitive

constructs associated with such adaptive and maladaptive regulation.

This paper is structured as follows: We first motivate the need for PRAD by identifying that a

large proportion of individuals representative of the general population demonstrate behavior

that is known to cause issues in traditional measurements of response inhibition, or demonstrate

behavior that highlights the needs greater process dissociation and mechanistic explanations of

behavior. We then demonstrate the adequacy of the PRAD model in explaining aggregate

patterns and individual level of behavior, show its added utility over cognitive models without

these dynamic mechanisms, and importantly, provide theoretical advances on the role of

proactive, reactive, and attentional mechanisms in cognitive control. We show how PRAD

allows debiasing inferences, improves our understanding of the role of adaptivity, our

understanding of individual differences, and ability to predict cognitive performance. We also

show the relevance of PRAD to understanding clinical subgroups, to our understanding of the

neural underpinnings of cognitive control, and to understanding the role of exposomic factors.

82   **Inhibitory Control and the Stop-Signal Paradigm**

Inhibitory control, the ability to withhold or cancel undesirable action, thought, and emotion, is

fundamental to goal-directed behaviors (Alderson, Rapport, & Kofler, 2007; Bonham, Shanley,

Waters, & Elvin, 2021; Lavagnino, Arnone, Cao, Soares, & Selvaraj, 2016; Lipszyc & Schachar,

2010; McTeague et al., 2017; R. Schachar & Logan, 1990; Smith, Mattick, Jamadar, & Iredale,

2014). The stop-signal task (SST, **Figure 1**) is a widely used paradigm (Frederick Verbruggen et

al., 2019; Verbruggen & Logan, 2008) to study inhibitory control mechanisms and their neural

underpinnings. The SST involves making a response to a *Go* signal but inhibiting the prepared

response when the *Go* signal is quickly followed by an infrequent *Stop* signal. The time interval

between Go and Stop signals is called the stop-signal delay (SSD) and is experimentally

manipulated. On stop signal trials with longer SSD, the prepotent Go response is cognitively

further along, and more difficult to stop after detecting the Stop signal. The SST has been used in

a variety of domains, including non-human primates (Ghasemian, Vardanjani, Sheibani, &

Mansouri, 2021; Godlove et al., 2011; Liu, Heitz, & Bradberry, 2009), rodents (Bari et al., 2011;

Caglayan, Stumpenhorst, & Winter, 2021; Eagle et al., 2009; Mayse, Nelson, Park, Gallagher, &

Lin, 2014), during development in children (Cai et al., 2019; Carver, Livesey, & Charles, 2001;

R. Schachar & Logan, 1990; Williams, Ponesse, Schachar, Logan, & Tannock, 1999), through

the adult human life span (Hsu & Hsieh, 2022; Tsvetanov et al., 2018), in neurodiverse

populations (Adams & Jarrold, 2012; Alderson et al., 2007; Bonham et al., 2021; Geurts, van den

Bergh, & Ruzzano, 2014; Schmitt, White, Cook, Sweeney, & Mosconi, 2018; Senderecka,

Grabowska, Szewczyk, Gerc, & Chmylak, 2012; Soreni, Crosbie, Ickowicz, & Schachar, 2009),

psychiatric disorders (F.-F. Li, Chen, Zhang, Li, & Li, 2021; Lipszyc & Schachar, 2010;

McTeague et al., 2017; Sjoerds, Van Den Brink, Beekman, Penninx, & Veltman, 2014; Yu et al.,

2022), under the effect of medication (Kalanthroff et al., 2017; Sarkar et al., 2020) and

intervention (Cai, George, Verbruggen, Chambers, & Aron, 2012; N. Swann et al., 2011; Wessel,

Diesburg, Chalkley, & Greenlee, 2022), substance dependence (C.-s. R. Li et al., 2008; C.-s. R.

Li, Milivojevic, Kemp, Hong, & Sinha, 2006; Smith et al., 2014), sleep disorders (Covassin et

al., 2011; Zhao et al., 2018), learning difficulties (De Weerdt, Desoete, & Roeyers, 2013;

Schmid, Labuhn, & Hasselhorn, 2011), eating disorders (Lavagnino et al., 2016; Svaldi,

Naumann, Trentowska, & Schmitz, 2014), in studies of pregnancy related changes (Fiterman &

Raz, 2019), and genetic basis of inhibitory control (Barnes, Dean, Nandam, O'Connell, &

Bellgrove, 2011).

Understanding the dynamic cognitive mechanisms that underlie SST holds great promise for

enhancing our knowledge of latent processes driving cognitive functioning. Despite its

widespread use however, the SST and the traditional computational models applied to interpret it

face significant challenges that limit their explanatory power and practical utility.

The most common approaches measure the efficiency of an individual's inhibitory control by

estimating the latent stop-signal reaction time (SSRT). SSRT cannot be measured directly and is

typically estimated using a theoretical race model (Logan & Cowan, 1984; Logan, Van Zandt,

Verbruggen, & Wagenmakers, 2014; Verbruggen & Logan, 2009a). Conventional methods for

estimating the SSRT are the mean method and the integration method. In the mean method

(mSSRT), the mean inhibition function or probability of responding given a stop signal during an

SSD (for details, see Logan and Cowan (1984); Verbruggen and Logan (2009a)) is subtracted

from the mean RT distribution. In the integration method (iSSRT), the completion of the stop

process is estimated by integrating the RT distribution and determining the point at which the

integral equals the probability of responding for a specific delay (Logan and Cowan (1984);

Verbruggen and Logan (2009a)). The mean or integrated SSRT are the primary non-parametric

methods used to index cognitive control, and the most popular measures used. Other measures

include the slope of the inhibition function (Verbruggen & Logan, 2009a), or bespoke model-

based measures of SSRT.

137   **Need for a comprehensive integrative theoretically-motivated modeling framework**

The need for a comprehensive, integrated, theoretically-motivated cognitive model stems from

(i) Traditional models and related measures of SSRT being inappropriate for a significant

proportion of individuals (**Figure 2**, green); **(ii)** Need for explanatory mechanisms – greater

cognitive process dissociation and mechanistic explanations of behavior (**Figure 2**, blue). Figure

2 is based on the ABCD study where we examined 7,787 children who completed two runs of

the SST task inside an fMRI scanner at baseline.

Traditional models and related measures of SSRT are not adequate or appropriate for a

significant proportion of individuals

The validity of inferred SSRT measures become more questionable in the presence of specific

behavioral patterns that confound SSRT measurement (R. A. Doekemeijer, Dewulf, Verbruggen,

& Boehler, 2023; Verbruggen, Chambers, & Logan, 2013; Weigard, Heathcote, Matzke, &

Huang-Pollock, 2019), potentially leading to systematic biases in conventional measures of

SSRT and inhibitory control. There is a consensus that traditional and non-parametric (such as

mean and integration methods) measures of SSRT should not be calculated or used when the

assumptions of the conventional race model are violated, or when certain patterns of atypical or

extreme behavior is observed. Recent research (Bissett, 2014; Bissett, Hagen, Jones, & Poldrack,

2021; Bissett, Jones, Poldrack, & Logan, 2021) has highlighted the severe implications of these

violations, questioning the use of non-parametric SSRT as a definitive measure of inhibitory

control (Bissett, Jones, et al., 2021; Verbruggen et al., 2013), although recent approaches have

proposed model-based solutions to overcome some of these issues (Weigard, Matzke, Tanis, &

Heathcote, 2021a, 2023). When non-parametric methods are used, the integration method

(iSSRT) is considered more reliable and less biased than the mean method (Frederick

Verbruggen et al., 2019). However, even iSSRT has been shown to have biases and

underestimate true SSRT under multiple conditions.

Violations of context or stochastic independence. Context independence refers to the

assumption that go process reaction time distributions do not depend on whether or not a stop

signal is observed, an assumption that is critical to non-parametric estimates of the SSRT. This

assumption however has been shown to be consistently violated in a variety of stop signal tasks

(Bissett, Jones, et al., 2021), including in the ABCD study (Bissett, Hagen, et al., 2021), where

7% of the participants show violations of context independence, as benchmarked by having stop

RTs that are longer than go RTs (Frederick Verbruggen et al., 2019). Analysis of the ABCD data

has shown that one important dimension of context dependence of the go process is the duration

of the go stimulus, which varies significantly between trials, and also between go and stop trials

on an average (Bissett, Hagen, et al., 2021), with stop trials having shorter stimulus display

durations because of the onset of SSD. Bissett, Hagen, et al. (2021) recommend that parametric

cognitive models of the stop signal task incorporate the sensitivity to stimulus duration into the

go process. One such implementation proposed by (Weigard et al., 2021a), targets stop trials,

such that the SSD affects the go process drift rate in a linear manner, until asymptotic

performance is reached on par with the drift rate estimated on go trials. This addresses one of the

issues raised, in terms of the large difference in stimulus presentation duration between stop and

go trials but may not directly account for variability in stimulus duration within go trials.

Stochastic independence refers to the assumption that the finishing times of go and stop

processes are independent on any trial, and violations of this assumption have been shown to

lead to biases in the accurate estimation of SSRT (Frederick Verbruggen et al., 2019). Violations

of stochastic independence might show up as high correlations between go process reaction

times and SSRT times. In terms of model-free behavioral assessments, this has been shown to

affect the slope of the inhibition function, that is, the rate of change in stop failure rate with

increasing stop signal delays. We arrive at a conservative model-free estimate that in the current

study, 5.2% of the participants may exhibit violations of stochastic independence, based on

benchmarking against previous simulation studies (**Methods**).

Higher skew and slowdown of reaction times. Higher right skew of the go process reaction

times has been shown to bias estimates of non-parametric SSRT (Frederick Verbruggen et al.,

2019; Verbruggen et al., 2013). Higher skew could be a sign of strategic or proactive slowing, or

other sequential effects that produce greater variability in reaction times. In the current study,

14.5% of participants demonstrated higher levels of skew (**Methods**). Higher slowing of go

process reaction times has also been shown to bias estimates of non-parametric SSRT (Frederick

Verbruggen et al., 2019; Verbruggen et al., 2013). Higher slowdown could also be a sign of

strategic or proactive slowing or other sequential effects. In the current study, 4.8% of

participants demonstrated higher levels of RT slowdown (**Methods**).

Deviations in stop success rates and go-omission rates. Higher go omission rates have been

shown to affect accurate estimation of non-parametric SSRT (Frederick Verbruggen et al., 2019).

Higher go omission rates may reflect some form of anticipatory preparation for inhibition before

the observation of a stop stimulus. In the current study, 8% of participants demonstrated higher

levels of go-omission rates (> 20%). Conventional non-parametric models also cannot capture

patterns of inhibition functions that vary with SSD (Bissett, Hagen, et al., 2021), and SSRT

estimates have also been shown to be unreliable when response inhibition (stop success rate)

deviates sharply from 0.5, especially with higher stop success rates (Frederick Verbruggen et al.,

2019). In the current study, 1.5% of participants demonstrated high deviations (SFR < 25% or >

75%).

Need for explanatory effects – greater process dissociation and mechanistic explanations of

behavior

Beyond just the ability to accurately measure SSRT for a diverse population with individual

differences, a large body of work has shown the influence of multiple cognitive processes on

inhibitory control, including proactive and strategic adjustments, sequential effects including

error-monitoring and related adjustments, and attentional mechanisms such as trigger failure of

the stop process. No existing model captures and measures all of these theoretically motivated

aspects in a single quantitative framework that can provide a mechanistic explanation of how

these components interact, and provide a measurement model for distinct cognitive process. The

most important of these is the need for a cognitive model of the proactive inhibitory mechanisms.

Most previous measurements of proactive inhibition have relied on bespoke experimental

manipulation, rather than a cognitive modeling approach that can be applied to standardized

experimental paradigms.

Ability to identify, measure, and explain proactive mechanisms. Existing models of inhibitory

control often fail to adequately differentiate between proactive and reactive control mechanisms.

Proactive control refers to the anticipation and prevention of impulsive actions through the

maintenance of goal-relevant information, whereas reactive control involves the suppression of

an action in response to a stop signal (A. R. Aron, 2011; T. S. Braver, 2012; Cai, Oldenkamp, &

Aron, 2011). The dichotomy between these processes and their interaction with both top-down

and bottom-up regulatory mechanisms remains insufficiently explored in current research

paradigms, especially in terms of quantitative measurements of such interacting processes (Adam

R Aron, 2011; Elchlepp, Lavric, Chambers, & Verbruggen, 2016). In the current study, 18.9%

participants demonstrated exceptionally high levels of variability in RT (**Methods**), suggesting a

possibility for mechanisms that modulated within-individual RT.

Proactive inhibitory control has been assessed in terms of response slowing and higher

variability (higher SD of RT) of the go process in blocks or cued designs when a stop signal is

present compared to those that have no stop signals. However, such assessment requires a

modified experimental setup and cannot be easily or directly assessed in a traditional stop signal

task. Previous studies have modified the standard SST paradigm to probe the proactive

component (Weidong Cai et al., 2023; Chikazoe et al., 2009; N. C. Swann et al., 2012;

Verbruggen & Logan, 2009b; Vink, Kaldewaij, Zandbelt, Pas, & du Plessis, 2015), introducing

variability in task design, and rendering replication more challenging. Such experimental setups

have shown that a simple diffusion model fit of the reaction times resulted in an increase in the

non-decision times for blocks that contain stop-signals (Verbruggen & Logan, 2009b). This has

been attributed to either delayed-processing, where the processing of the go stimulus may be

delayed, or response-suppression, where motor output is temporarily suppressed. Existing data

are often compatible with both hypotheses. It might be expected that the 'excess' non-decision

time inferred in such situations is independent of SSD and relatively stable in the latter

hypothesis, but shows greater variability and depends on some learning-based expectancy of

SSD in the delayed-response hypothesis. This need for SSD tracking of the delayed response

hypothesis has led to some suggestions that it may be cognitively difficult to implement. It has

however been suggested that SSD values could affect general strategy shifts in the stop signal

task (Bissett, Hagen, et al., 2021), and that SSD and expected probability of stopping can affect

reaction times (Ma & Yu, 2015). Some recent work (Elchlepp et al., 2016; Hu & Li, 2012; Perri,

2020) has also suggested that these response focused views should be expanded to include the

role of dynamic attention in proactive control, including trial by trial modulation of attention and

response settings, and a general attentional inhibitory account. This is also supported by evidence

(Lee & Kang, 2020) that even proactive inhibition may employ distinct mechanisms that

dissociate influence on slower reaction times and lower erroneous responses, suggesting that a

simple adjusted-response threshold based explanation of proactive inhibition (Elchlepp et al.,

2016) may not be sufficient. In addition, there is mixed evidence that proactive inhibition may

support better reactive inhibition (Castro-Meneses, Johnson, & Sowman, 2015), suggesting some

form of interaction between these processes.

Existing accumulator based cognitive models of the stop signal paradigm do not capture the

possibility of variable SSD dependent delayed processing contributing to proactive inhibitory

control or attention modulation (beyond rates of trigger failure, which are SSD independent),

although there have been models proposed that capture similar dynamic belief effects within a

Bayesian optimal control model (Ma & Yu, 2015). Such dynamic belief models have been used

to study proactive control in the SST (Cai, Chen, Ide, Li, & Menon, 2017; Ide, Shenoy, Angela,

& Chiang-Shan, 2013), but do not simultaneously incorporate other latent components, such as

reactive control (Shenoy & Yu, 2011). They do not incorporate an evidence accumulation

mechanism and have not typically been used as measurement models. They have been used

primarily to showcase the influence of dynamic experimental contingencies (such as probability

of stopping and SSD) on the variability of reaction times across subjects, without modeling any

individual level parameterization that can capture or measure individual differences. Moreover,

this class of models assumes an optimal Bayesian process, and are not ideal to model impaired

processes or variations in clinical populations. This theoretical gap hinders a comprehensive

understanding of the multiple dimensions of inhibitory control and their implications for

behavior and cognition. There is thus, a need for cognitive models that capture processes in an

integrated manner, the effect of SSD tracking on inhibitory modulation, possible mechanisms of

proactive inhibition in the form of delayed response or response suppression, and the modulatory

effects of preemptive mechanisms on reactive inhibition.

Sequential effects affecting the go process. We measured whether the reaction times or go-stop

errors differed between trials that followed a correct or incorrect trial (incorrect trials included go

omissions or stop failures). 48.8% of participants showed significant differences in at least one of

these measures, and 33.8% showed significant differences specifically in reaction times,

demonstrating the influence of error-based sequential effects on the go process. This sequential

effect demonstrates another form of stochastic dependence, and motivates the need for

mechanisms that explain systemic patterns of intra-individual variability without assuming that

the go process is independent and identically distributed (IID) across trials. In addition, response

thresholds have been shown to increase post errors and result in post error slowing in a variety of

tasks (Schroder et al., 2020), but these mechanisms are not usually incorporated into cognitive

models of the stop signal task. 6.4% of participants in this study demonstrated statistically

significant post-error slowing.

Sequential effects affecting the stop process. Apart from the go process, stopping processes may

also not be context independent, conditional stop trial probabilities may influence behavior, and

SSRT may depend on SSD (Bissett, Hagen, et al., 2021). These aspects remain unaccounted for

in most known cognitive models of the stop signal task that employ evidence accumulation

models. Modulation of the conditional probability of stopping has been incorporated in some

other models (Ma & Yu, 2015) but not explicitly as attentional mechanisms that depend on the

number of trials that have elapsed since the last stop signal was encountered. 11.2% of

participants showed a significant correlation between the number of trials since a stop signal was

last observed, and the stop failure rate, demonstrating some sequential attentional mechanisms

affecting dynamic modulation of the stop process.

Given the issues with non-parametric estimation of SSRT, alternate methods for estimation of

SSRT are parametric models, which may be cognitive, statistical, or hybrid models that model

the decision-making process within the SST paradigm. Some of these models are based on

assumptions of a parametric distributional form of the SSRTs (Matzke et al., 2013; Weigard et

al., 2019; Weigard, Matzke, Tanis, & Heathcote, 2021b). Others are based on the assumption of

competing evidence accumulator processes reflecting plausible cognitive mechanisms

(Heathcote & Love, 2012; Logan et al., 2014). However, the stop signal evidence accumulation

process within such models has been shown to have poor identifiability and thus not be a suitable

measurement model (Matzke, Logan, & Heathcote, 2020a). As an alternative, hybrid models

have been suggested where the go process is modeled by a cognitive evidence accumulation

process, and the stop process characterized by a parametric distribution such as the ex-Gaussian

distribution (Weigard et al., 2021b). While such methods have produced more reliable and useful

estimates of SSRT, they may not be the most suitable approach for accounting for how an

integrated set of cognitive processes such as belief updating, error-based learning and

modulation, and adjustment of attentional and response parameters affects the stop process in a

dynamic manner.

Mechanisms underlying trigger-failures of the stop process. In previous literature it has been

empirically observed that stop failure rate sometimes does not approach zero even on extremely

short SSDs close to zero, and this has typically been explained with the assumption of trigger

failures (R. Doekemeijer, Verbruggen, & Boehler, 2021), that is, a failure of the stopping process

to initiate on a small subset of stop trials. Without the concept of trigger failures, it would be

required that a stopping process that generates short enough SSRTs to work effectively at higher

SSDs would also produce extremely long SSRTs that fail to successfully inhibit action at SSDs

close to zero. Traditional models with fixed SSRTs, or even those that allow random variability

in SSRT cannot produce the high level of trial-level variability required to consistently explain

these findings at low and high SSDs. Some models (Matzke, Love, & Heathcote, 2017) have

thus been augmented with a trigger-failure mechanism that assumes that the stop process fails to

initiate on some percentage of stop trials. The inferred failures of inhibitory response processes

have been associated with impulsivity (Skippen et al., 2019). It has also been proposed that there

may be a confound between trigger failures and inference of longer SSRTs (Weigard et al.,

2019). Allowing for a high-variability stopping process that can account for shorter and longer

SSRTs, and thus provide an underlying systemic mechanism for when behavior that seems like a

trigger-failure occurs, can provide a more powerful understanding of the dynamic mechanisms

modulating the stopping process. In this study, 7.4% of the participants had stop failure rates in

the lowest 10th percentile (shortest or easiest SSDs) that were at least as high or higher than in

the highest 10th percentile (longest or hardest SSDs), representing participants for whom

mechanisms similar to, or underlying trigger failures may be relevant.

Summary

Typical recommendations (Bissett, Hagen, et al., 2021) to capture accurate inhibitory capacities

based on the independent race model focus on excluding participants with extreme behaviors, or

focus on experimental design that encourages standardized behavior – minimizing strategic

adjustments, slowing, sequential effects, etc. These approaches reduce the elicitation of

individual differences, and try to minimize the role of multiple cognitive and metacognitive

systems that interact with core reactive inhibitory capabilities. Capturing individual differences

in these multiple cognitive and metacognitive systems is critical for understanding behavior in

ecologically relevant cognitive control situations. In the current study, using the above defined

conservative benchmarks, at least 32.6% (**Figure 2**; green) participants show at least one of the

behaviors outlined above that will affect accurate estimation of non-parametric SSRT.

Additionally, at least 65.2% (**Figure 2**; blue) of participants demonstrate the need for at least one

of the dynamic measures of individual differences outlined above – in proactive mechanisms or

sequential dependencies in go or stop processes, that interact with and complement basic reactive

inhibitory control. Overall, 74.3% of participants fall under at least one of the above two

categories. Note that some of these estimates are made based on subjective criteria (**Methods**).

Nonetheless, it is not the specific proportions that are important, rather the fact that a substantial

proportion of participants demonstrate these.

This critique underscores a critical gap in the current understanding and measurement of

inhibitory mechanisms, pointing to the need for more quantitively precise models that can

account for the complex dynamics of cognitive processes. To address this, we develop,

implement, and validate a model of Proactive, Reactive, and Attentional Dynamics (PRAD), a

novel computational cognitive model for inhibitory control that comprehensively accounts for

the multi-componential dynamic processes that are not currently represented in extant models,

and can address most of the above issues (see **SI Table S1** for a complete list of features).

Proactive, Reactive, and Attentional Dynamics (PRAD) - An Integrated Approach

The PRAD model incorporates the dynamic modulation of behavior by multiple latent cognitive

processes governing inhibitory control, allowing for multiple forms of sequential dependencies,

both in the go and stop processes, and provides quantitative measurements for multiple cognitive

components of reactive and proactive control. The dynamic modulation of behavior is based on

theoretically motivated processes and includes dependencies on both endogenous (cognitively

generated, such as being based on error-monitoring) and exogeneous (experimental

contingencies, such as updating beliefs based on varying stop signal delays, or attentional

modulation based on the number of trials since a stop signal was encountered) variables.

Importantly, it allows for measurement of individual differences in the cognitive variables that

govern how these sequential dependencies are operationalized. PRAD does not require

assumptions about context or stochastic independence, and it is not constrained by behavioral

patterns such as high skewness of slowdown in reaction times, or extreme error rates that impact

robust measurement of SSRT in traditional approaches. It provides a novel comprehensive

account of dynamic reactive and proactive inhibition, providing more robust and dissociated

measures of individual differences in inhibitory control. We demonstrate PRAD's robustness

across a wide range of measures and test its ability to overcome limitations of conventional race

models.

One of our key objectives of implementing PRAD was to make theoretical advances in our

understanding of cognitive control dynamics, by examining the distinct components of inhibitory

control, including proactive delayed response (PDR) mechanisms (**Figure 3A**; green box) and

attentional modulation of stopping (AMS) mechanisms (**Figure 3A**; yellow box), and their

dynamic interactions, and by investigating systemic intra-individual variability in inhibitory

control processes. A second key objective was to provide debiased estimates of SSRT, and

debias inferences about cognitive control mechanisms especially for typically underrepresented

or atypical populations. Since PRAD provides a multidimensional measurement system, this is

expected to provide a stronger characterization of individual differences. Our third objective

focused on evaluating the relevance of PRAD measures to a variety of cognitive task

performance measures, its relevance to identifying differences in clinical subgroups, its ability to

identify specific neural mechanisms underlying proactive and reactive control, and its relation to

exposomic factors (Moore et al., 2022). These goals sought to validate PRAD's effectiveness

beyond its initial context and explore its potential as a more precise tool for understanding the

latent substrates of cognitive variability. We leverage the large-scale, Adolescent Behavioral and

Cognitive Development (ABCD) study data to develop and test the PRAD model in a

developmentally homogenous (ages 9-10) group of children who completed the SST task.

Specification of the PRAD model

The PRAD model was implemented within a hierarchical Bayesian framework, allowing for the

estimation of both individual-level parameters and trial-level measures. This approach enables

the identification and measurement of distinct components that characterize individual

differences in inhibitory control, while also accounting for the temporal variability in cognitive

processes. **Figure 3A** illustrates the model's structure, incorporating proactive, reactive, and

attentional mechanisms. **Figure 3B** and **SI Table S2** illustrate the mechanisms and summarize

the key model parameters.

Competing Go and Stop processes. Overall, the PRAD model incorporates separate evidence

accumulation (drift-diffusion) processes for the go and stop processes, similar to a canonical

horse-race model (Band, Van Der Molen, & Logan, 2003). However, in addition to typical drift-

diffusion process parameters, PRAD includes additional individual trait-like and dynamic trial-

level measures, which have been shown to improve model inferences in different cognitive tasks

(Mistry, Chang, El-Said, & Menon, 2025; Mistry, Skewes, & Lee, 2018; Mistry & Trueblood,

2015).

Dynamic modulation of the Go process (PDR). The go process is modeled as a drift diffusion

process, modulated by a probabilistic proactive delayed responding (PDR) mechanism, which in

turn, is driven by a cognitive state switching mechanism and belief updating about stop signal

delays. On proactive trials, the go process can be strategically delayed in anticipation of a

possible stop signal. In PRAD, ρ_t is a binary variable representing the presence ($\rho_t = 1$) or

absence ($\rho_t = 0$) of a proactive cognitive state on trial t. The proactive delayed responding is

only initiated on proactive cognitive states. Proactive cognitive states are governed by a baseline

proclivity for proactivity (θ_0), and performance-monitoring based modulation (θ_1).

444
$$\rho_t \sim Bernoulli\left(\frac{1}{1 + e^{-\left(\theta_0 + \theta_1\left(\epsilon_{G,t-1}\right) - \theta_1\left(\epsilon_{S,t-1}\right)\right)}}\right).$$

Here, $\epsilon_{G,t-1}$ is an indicator of a go-omission (incorrectly stopping on a go trial) on the previous

trial, and $\epsilon_{S,t-1}$ is an indicator of a stopping error (not stopping on a stop trial). The PRAD

model assumes that the correction in terms of increasing or decreasing the probability of a

proactive cognitive state following these two types of trials will be in opposite directions. The

sign of θ_1 is an indicator of adaptivity or maladaptivity of the performance monitoring

mechanism – when θ_1 is negative, ρ_t adaptively increases after a stop-failure but reduces after a

go-omission, and when θ_1 is positive, ρ_t maladaptively decreases after a stop-failure but

increases after a go-omission. The absolute value of θ_1 is the sensitivity of the state-switching

mechanism to errors and governs how large of an effect the errors have on the trial-level

probability of proactivity. The probability of proactivity in the model is the posterior mean of ρ_t,

i.e., the posterior probability of $\rho_t = 1$.

When in a proactive cognitive state, the onset of the go process may be deliberately delayed in

anticipation of a stop signal. This dynamic adaptation is modeled by adding a further delay ω_t to

the go process to reflect proactive delayed responding to the go stimulus, where:

$$\omega_t = \lambda_t \, \rho_t.$$

Here, λ_t reflects a trial-level belief updating process, based on the history of stop signal delays

(SSD) encountered, and is an internal noisy estimate of the prospective anticipated SSD. The

parameter μ ($0 < \mu < 1$) reflects persistence in belief updating, with high persistence implying a

lower decay rate of older SSDs encountered. Further, letting SSD_t be the SSD on trial t and $\mathbb{I}_{S,t}$

be a stop trial indicator on trial t, the belief updating can be written as:

$$\lambda_t = \frac{\left(\sum_{i=1}^{t-1} \mu^{t-i-1} \, \text{SSD}_i \, \mathbb{I}_{S,i}\right)}{\left(\sum_{i=1}^{t-1} \mu^{t-i-1} \, \mathbb{I}_{S,i}\right)}.$$

Proactive delaying (ω_t) is the posterior mean of λ_t on trials with probability of proactivity

greater than 0.5, otherwise 0. Thus, the overall effective non-decision time, as compared to

traditional models, will be:

$$\tau_G + \omega_t$$

Here, τ_G is the trial-invariant or core non-decision time component, while ω_t measures the

strategic adjustment to the non-decision time. Note that because of this mechanism, τ_G cannot

directly be compared to non-decision times from traditional models (see **Methods** for details).

In addition to the PDR mechanism, the go process incorporates a trial-varying decision threshold

($\alpha_{G,t}$) and drift rate ($\delta_{G,t}$). The dynamic decision threshold is based on post-error adjustments:

482   $$\alpha_{G,t} = \alpha_{G1}\left(1 - \epsilon_{C,t-1}\right) + \alpha_{G2}\left(\epsilon_{C,t-1}\right),$$

where (α_{G1}, α_{G2}) are distinct threshold levels and $\epsilon_{C,t-1}$ is an indicator of whether the left vs

right choice on the previous trial was erroneous. Thus, the dynamic threshold implements a form

of performance monitoring and varies between two levels based on the outcome of the previous

trials, with α_{G1} being the default threshold and α_{G2} reflecting the threshold after post-error

adjustments.

The dynamic drift rate is specified as:

496   $$\delta_{G,t} = \frac{\delta_0\ \mathbb{S}_{LR,t}}{\left(1 + e^{-12(stim_t - \kappa_0)}\right)} \ \text{if}\ stim_t \neq 0, \text{else } 0.$$

Here δ_0 is a measure of the maximum drift rate for an individual, with the actual drift rate

depending on the duration of the go stimulus ($stim_t$) and an individual parameter κ_0, which can

be interpreted as the stimulus duration at which the drift rate is half the maximum. $\mathbb{S}_{LR,t}$ assumes

values 1 or -1 depending on the direction of the go stimulus (left or right). PRAD allows for trial

level changes to the drift rate, overcoming the issues with variable go stimulus durations

highlighted in previous work (Bissett, Hagen, et al., 2021), especially on stop trials where the go

stimulus is overridden by the stop signal. Since the duration of the go-stimulus on go trials is

confounded with the RT, making this a discriminative rather than generative model, we also test

a fully generative model (PRAD-g; see **Methods** for details), where the dynamic drift rate is only

applied on stop trials, and on go trials, it is retained as $\delta_0\ \mathbb{S}_{LR,t}$, similar to previous work

(Weigard et al., 2023).

The reaction times of the go process correspond to the reaction times for pressing the left or right

buttons in response to the go stimulus.

Dynamic modulation of the Stop process (AMS). The stop process combines baseline reactive

inhibition with attentional modulation of stopping (AMS). It is modeled as a drift diffusion

process with a trial-invariant non-decision time (τ_S), decision threshold (α_S), and drift rate (δ_S),

but a trial-varying bias ($\beta_{S,t}$). The stop process begins at the onset of the stop signal. The initial

bias is

505
$$\beta_{S,t} = \left(\frac{1}{1 + e^{-\gamma_1(nSSD_t - \gamma_0)}}\right).$$

Here, $nSSD_t$ reflects the number of trials since a stop signal was last encountered. This reflects

an attentional mechanism that modulates the stopping bias $\beta_{S,t}$ (which varies from 0 to 1).

Positive values of γ_1 result in an increase in stopping bias as $nSSD_t$ increases and vice versa.

Similarly, negative values of γ_1 result in a decrease in stopping bias as $nSSD_t$ increases and vice

versa. The absolute value of γ_1 measures the sensitivity to attentional modulation. The γ_0

parameter is a measure of the value of $nSSD_t$ when stopping bias is neutral (0.5).

The reaction times of the stop process correspond to the SSRT. The stop process is only initiated

on stop trials after the appearance of the stop stimulus (which appears after a delay

corresponding to the SSD). The PRAD model thus allows SSRT distributions to be dependent on

the stopping bias (conditional probability of stopping), which are in turn inferred to be

modulated based on attentional sensitivity to the number of trials that have elapsed since the last

stop signal was encountered. The SSRT is not manifested as a behavioral action. Rather, if the

SSRT, which is the duration of the stop process, plus the SSD on a stop trial is smaller than the

go process reaction time, then the go action can be successfully inhibited (successful stop). The

PRAD model enables obtaining the full posterior distributions of SSRT (Matzke et al., 2013), at

a trial level, rather than a single individual level estimate obtained using non-parametric

methods.

Model implementation. We implemented PRAD within a hierarchical Bayesian modeling

framework in JAGS (Plummer, 2003), which implements a Gibbs sampler for Markov Chain

Monte Carlo (MCMC) simulations. Both the go and stop processes are modeled using the

Wiener distribution (Wabersich & Vandekerckhove, 2014), which produces a joint distribution

of the reaction times and the decision choice on each trial. The sampling hyperparameters,

Bayesian priors, parameter recovery (**SI Figure S1**), and additional computational details are

described in the **Methods** section. We applied PRAD to SST data from 7787 individuals from

the ABCD dataset.

Control Models and Sensitivity Analysis. We also compared PRAD versus two control models

– fixed stopping model (FSM) and random variability model (RVM). Both of these include

competing go and stop processes, but FSM does not incorporate any trial-level variability in

SSRT, while RVM allows random variability in SSRT across trials. Neither incorporate PDR or

AMS mechanisms. In addition, we conducted a sensitivity analysis with slightly different

implementations of the PRAD model to test robustness to some modeling assumptions (PRAD-n,

PRAD-g, as well as subsampling based on choice of MCMC hyperparameters). Details are

provided in the **Methods**.

Model Validation - Explaining Aggregate Behavioral Patterns

PRAD demonstrated robust performance across various measures and outperformed control

models (**Figure 4A-F; SI Figure S2**). **SI Table S3** shows key observed measures at an aggregate

level, and the summarized PRAD model posterior values corresponding to these observed

measures.

At the group level, PRAD accurately captured trends in stop failure rates and reaction times

across different experimental contingencies (SSD, nSSD). Specifically, the posterior predictives

generated by the PRAD model explained aggregate behavioral patterns including non-linear S-

shaped patterns of stop failure rate with increasing SSD (**Figure 4A**) and non-monotonicity at

low SSD values, an indicator of violations of context independence (Bissett, Hagen, et al., 2021).

Importantly, unlike control models, PRAD effectively captured the diverse patterns across

different behavioral subgroups based on simple observed measures, such as whether SFR

increased or decreased with SSD (**Figures 4C,E**). PRAD captured the increasing variability in

stop failure rate with the numbers of trials since encountering the last stop signal (nSSD), with

superior model fits for subgroup showing increasing and decreasing trends, both of which the

control models struggled to fit well (**Figure 4B,D,F**). This demonstrates the fewer inductive

biases within the PRAD model. PRAD also captured the linear increase in stop-failure RT with

increasing SSD (**SI Figure S2A**), an indicator of the link between slower RT and better stopping

performance, or the influence of SSD on RT, the increasing variability in RT with SSD (**SI**

Figure S2B), and lower choice accuracies at low SSDs (**SI Figure S2C**).

Crucially, the PRAD model outperformed both control models (FSM, RVM) on all of these

aggregate measures. RMSE distance from the observed aggregate curves (**Figure 4G, SI Table**

S4) show that across trends based on different experimental contingencies, PRAD reduced

RMSE of model fits by between 77% - 80% for SFR, 13% - 45% for RT on stop failures, and

48% - 61% for choice accuracies on stop failure, compared to the FSM model. Similarly, PRAD

reduced RMSE by between 58% - 66% for SFR, 45% - 50% for RT on stop failures, and 48% -

51% for choice accuracies on stop failure, compared to the RVM model. These results suggest

that incorporating sequential adaptive processes is crucial for characterizing behavioral dynamics

on the SST, which PRAD achieves better than conventional approaches.

Model Validation – Capturing individual differences and individual level behavior

We then examined PRAD robustness at the individual participant level. We assessed how well

the model posterior values generated by PRAD explain behavioral patterns at an individual level

(mean values per individual). Individual subject-level fits showed strong correlations between

PRAD model fits and observed data for multiple behavioral measures (**SI Figures S3**). Notably,

individual-level comparisons showed stronger correlations (**Figure 4H; SI Table S5**) and lower

RMSE (**SI Table S6**) between observed and predicted values for PRAD across almost all key

measures compared to the RVM and FSM control models. This included go reaction time (r =

0.91; p < 0.0001), stop-failure reaction time (r = 0.90; p < 0.0001), and stop-failure rate (r = 0.85;

p < 0.0001), but importantly, also second order effects like post-go RTs (r = 0.92, p < 0.0001),

post-stop RTs (r = 0.86, p < 0.0001), difference between stop and go RTs (r = 0.51, p < 0.0001),

post-inhibitory differences in RTs (r = 0.45, p < 0.0001), and dynamic within-subject

correlations like SFR vs SSD (r = 0.63, p < 0.0001) and SFR vs nSSD (r = 0.73, p < 0.0001).

PRAD's ability to account for the wide range of variability and individual differences is also

reflected in the Kullback-Leibler divergence between the distribution of observed measures and

model fit posterior values of these measures. PRAD reduces the KL divergence (thus providing a

closer match to the observed range of individual differences) for observed distributions by

between 29%-89% compared to RVM and 4%-83% compared to FSM (**SI Table S7**). These

results demonstrate that PRAD can accurately capture behavioral variability at both the

individual-subject level and in terms of individual differences between subjects.

Additionally, we measured Deviance information criteria (DIC), which assesses model fit

appropriately penalized for model complexity. In spite of the additional complexity, PRAD

resulted in lowest (best) DIC values for 60% of the individuals, compared to 22% for the RVM,

and 18% for the FSM model, suggesting that the additional complexity was necessary to explain

behavior in a majority of individuals.

Model Validation - Capturing intra-individual variability

For a significant proportion of participants, observed and latent measures show within-subject

correlations with various sequential or experimental contingencies **(SI Table S8)** such as SSD,

number of trials since the last stop signal was encountered (nSSD), the average SSD encountered

so far (xSSD), whether a left versus right error was made on the previous trial ($post_{CE}$), whether

the previous trial was a successful go versus stop trial ($post_{GSE}$), and whether the previous trial

was an inhibitory trial ($post_S$). 81% of the participants had a significant correlation of observed

trial-level RT, 95% had a significant correlation of observed trial-level go-stop errors, and 82%

had a significant correlation of latent trial-level SSRT with at least one or more of these

exogeneous (SSD, nSSD, xSSD) or endogenous ($post_{CE}$, $post_{GSE}$, $post_S$) variables. This analysis

suggests that a good cognitive model should be able to at least partially capture structural sources

of trial level intra-individual variability (IIV).

Analysis of IIV in Go RTs and SSRTs revealed that significant variance could be explained by

model parameters, rather than random noise (**SI Figures S4**). See **SI Table S9** for summary

statistics for PRAD latent dynamic measures, their coefficient of variation, and within-individual

95% CI ranges. We measured the partitioned variance of RTCV and SSRTCV into model

parameters that were theoretically relevant. This revealed that 72% of RTCV was explained by

the relevant cognitive model parameters. Of this, 26% was explained by standard drift diffusion

model parameters and interactions between them, 46% was explained by the novel adaptive

model parameters or their interactions with standard parameters, with 28% being residual,

attributed to unexplained IIV, and possibly the contribution of noisy cognitive processes to IIV.

Similarly, the partitioned variance of SSRTCV into relevant cognitive model parameters

revealed that 81% of SSRTCV was explainable. Of this, 40% was explained by standard drift

diffusion model parameters and interactions between them, 41% was explained by the novel

adaptive model parameters or their interactions with standard parameters, with 19% being

residual. These results point to the fact that a large percent of IIV can be explained structurally

by the cognitive model parameters, without resorting to random effects across trials.

Examining Model Dynamics With An Example

To visualize the dynamic interplay of key PRAD components and their trial-by-trial variability at

the individual subject level, we examined detailed time courses of model-derived measures for

representative participants. **Figure 5** illustrates the dynamics involved in stop trials from a single

participant, showing how stopping expectancy, SSRT, PDR, and RT interact on a trial-by-trial

basis. Stopping expectancy, modulated by attentional regulation, fluctuated considerably from

trial to trial and showed an inverse relationship with SSRT. This revealed how dynamic

attentional processes can influence inhibitory performance on a moment-to-moment basis. We

also observed that task difficulty (represented by SSD) and stopping efficiency (SSRT) varied

substantially across trials, with their sum (SSD+SSRT) providing insight into the overall

challenge of inhibition on each trial. Our analysis of stop-failure trials revealed complex

relationships between PDR, SSD+SSRT, and RT, demonstrating how proactive and reactive

mechanisms interact to determine inhibitory outcomes.

To further elucidate these dynamics, we closely examined three specific stop trials with varying

levels of difficulty. We found that successful inhibition could occur even on more difficult trials

(higher SSD) when compensatory mechanisms like increased stopping expectancy or heightened

PDR were engaged. Conversely, easier trials could result in failures when these compensatory

mechanisms were absent.

These observations highlight PRAD's capacity to capture and explain the substantial intra-

individual variability in inhibitory control processes, accounting for the complex interplay

between task parameters, attentional modulation, and proactive control strategies that occur on a

trial-by-trial basis.

658   **PRAD Advances Theoretical Perspectives of Cognitive Control**

Distinct cognitively plausible components of inhibitory control

The model envisages a core reactive inhibitory process, modulated by attentional variations in

stopping expectancies, and a dynamically adjusted proactive delayed response of the go process,

all three of which affect observed inhibitory behavior (**Figure 6A**). Factor analysis of a subset of

model parameters that are theoretically relevant to these three aspects of inhibitory control

revealed the robustness of this three-factor structure (CFI 0.997, TLI 0.977, RMSEA 0.045;

Figure 6B, SI Table S10). Factor 1, representing proactive control, loaded heavily on

parameters $(\theta_0, \theta_1, \mu)$ that governed the trial level probability of engaging PDR mechanisms, and

the adaptive belief updating about historical stop-signal delays that modulated the PDR duration.

Factor 2, capturing basic reactive control (baseline SSRT), was dominated by parameters (δ_s, α_s)

governing the baseline stop process. Factor 3, reflecting attentional modulation that influences

variations in trial-level SSRT, loaded strongly on parameters (γ_0, γ_1) influencing the dynamic

adjustment of stopping expectancy, which in turn affects dynamic SSRT. Factors 1 and 3 were

not correlated, but factor 2 shows low correlations with the other 2 factors ($|r| = 0.085, 0.16$; both

$p < 0.0001$), suggesting related but distinct processes. **SI Table S11** reports control analysis

showing that 1- and 2-factor models were not adequate, and a 4-factor model was not

identifiable.

The three factors explained a significant portion of individual differences in inhibitory control

performance. Regression analyses using all individual-level model parameters significantly

predicted various measures of inhibitory control, including PRAD stop-signal reaction time

(SSRT; $R^2 = 86\%$), observed stop-failure rate (SFR; $R^2 = 65\%$), observed mean experienced

stop-signal delay (xSSD; $R^2 = 77\%$), SSRT coefficient of variation (SSRTCV; $R^2 = 89\%$), as

well as observed RT ($R^2 = 67\%$) and RT CV ($R^2 = 68\%$), all p < 0.0001. Importantly,

parameters from each of the three factors contributed uniquely and significantly to these

predictions, with standardized beta coefficients ranging from -0.86 to 0.80 (see **SI Table S12**).

These results align with the theoretical constructs of proactive control, reactive control, and

attentional modulation, and validate the model's ability to dissociate different aspects of

inhibitory control, thus representing distinct cognitive pathways that they can be dissociated into

distinct components characterizing individual differences. They demonstrate that PRAD is a

robust cognitive framework for distinguishing among three dissociable pathways of response

inhibition beyond reactive control alone (Hu & Li, 2012; Lee & Kang, 2020; Perri, 2020), and

contribute towards the development of a richer theoretical framework (Mirabella, 2023).

Proactive Mechanisms

PRAD revealed the substantial contribution of PDR mechanisms to inhibitory control. Across

individuals, proactive cognitive states occurred on an average of 78% of trials (2.5th to 97.5th

percentile 3-98%), with PDR accounting for approximately 28% (2.5th to 97.5th percentile 2-

51%) of average reaction times of 515ms (mean PDR = 150ms, 2.5th to 97.5th percentile 8-

322ms; **Figure 7A**).

Between subjects, the average PDR is associated with both the mean RT (r = 0.59, p < 0.0001) of

responses as well as RTCV across trials (r = -0.51, p <0.0001), and is negatively correlated with

SFR (r = -0.59, p < 0.0001), and positively correlated with xSSD (r = 0.61, p <0.0001). The

variability in PDR (PDRCV) is correlated with RTCV (r = 0.36, p <0.0001). Linear regressions

(**SI Table S13**) show that across individuals, PDR is significantly related to SFR ($R^2 = 0.48$,

$\beta = -0.44, \ p < 0.0001$) and xSSD ($R^2 = 0.46, \ \beta = 0.48, \ p < 0.0001$) even after controlling

for SSRT. The results demonstrate that individuals with longer delayed responding show more

successful inhibitory control (lower SFR, higher xSSD) by appropriate modulation of RTs, even

after controlling for the effect of SSRT on successful inhibition. Regression controlling for the

influence of average experienced SSD and SSRT shows that the average probability of proactive

states is significantly related to SFR ($R^2 = 0.65, \ \beta = -0.15, \ p < 0.0001$). Within-subject

regressions also show that after controlling for SSRT, SSD, and variable drift rate across trials,

the probability of proactivity, but not the length of proactive delay, is significantly related to

stop-failures (**SI Figure S6**).

Higher baseline proactivity (θ_0) was positively associated with increased PDR (r = 0.44, p <

0.0001) but not so with RT (r = -0.07, p<0.0001), suggesting that PDR mechanisms may be

linked to core capabilities, and individuals with faster processing speeds may also have improved

top-down PDR regulation. Baseline proclivity for proactive control (θ_0) is also correlated to

lower RT coefficient of variability (r = -0.29, p <0.0001).

Crucially, longer proactive delays were associated with more successful inhibition, underscoring

the pivotal yet underappreciated role of proactive control in SST performance. This echoes a few

previous findings that revealed negative association between proactive control and SSRT and

suggested that better proactive control is related to faster stopping speed (Cai, Mizuno, Tomoda,

& Menon, 2023; Chikazoe et al., 2009). It is noteworthy that these previous studies relied on

additional experimental manipulation to probe proactive control whereas PRAD can identify

proactive control components from the standard SST. Such studies with experimentally

manipulated versions of the SST task have estimated go response delays in the range of 100-

140ms (Castro-Meneses et al., 2015; Chikazoe et al., 2009; Jahfari, Stinear, Claffey, Verbruggen,

& Aron, 2010), similar to the PRAD inferred average of 150ms

These findings have important implications. Previous models largely focused on reactive control,

which is important for responding to unexpected stimuli in the environment. However, many

daily life situations require proactive control to minimize the need for reactive inhibition and

reduce impulsivity. As proactive control is generated by an individual's goals, explicit

measurements of it may have greater ecological validity in characterizing everyday response

tendencies and psychopathology.

Error-monitoring and adaptive or maladaptive modulation of proactive states

PRAD reveals selective proactive slowing (delayed responding) of the go process on some trials

governed on a baseline propensity for proactivity that is adaptively (or maladaptively) modulated

at a trial-level based on error monitoring. Adaptive modulation would involve increasing the

probability for proactive slowing after failing to inhibit responses on a stop signal trial, and

reducing it after an omission on a trial with no stop signal. Maladaptive modulation would work

in the opposite direction. The direction and magnitude of error-monitoring based modulation of

this probability based on whether the previous trial was a stop-failure or go-omission is

operationalized by the θ_1 parameter. A higher negative value is optimal, a value close to zero

implies no modulation based on error-monitoring, whereas a positive value implies maladaptive

modulation. In the latter case, the probability for proactive slowing, would counter-intuitively, be

increased after a go-omission and decreased after a stop-failure.

Figure 8A illustrates two actual participants with different values of θ_1. The first, with a high

baseline propensity for proactivity, shows how adaptive modulation (θ_1 = -2.42) helps shift

towards non-proactive states after go-omissions. The second, with a low baseline propensity for

proactivity, shows how maladaptive modulation (θ_1 = 2.02) helps shift towards proactive states

after go-omissions. **Figure 8B** shows how individual differences in participants' error-based

modulation affect changes in the probability of proactive. For individuals with $\theta_1 < 0$ (62% of

individuals) the average probability of proactive response states post stop-failure increases

adaptively to 90% compared to 73% post go-omission (**Figure 8C**). For individuals with $\theta_1 > 0$,

this maladaptively reduces to 54%, compared to 77% post go-omission. The resulting differences

manifest as a difference in reaction times (since proactive slowing increases RT), between post

stop-failure and post go-omission trials. This difference depends on whether individuals

demonstrate adaptive ($\theta_1 < 0$; mean RT increase of 37ms) or maladaptive ($\theta_1 > 0$; mean RT

decrease of 25ms) error-monitoring. Higher values of θ_1 lead to higher go-omission rates (r =

0.527, p < 0.0001), and lower values of θ_1 lead to higher post-inhibitory error effects, with a

negative correlation between θ_1 and the difference between post-stop error and post-go error RTs

(r = -0.38, p < 0.0001).

This component of PRAD can be construed as engaging error-monitoring and executive function

systems, and effecting top-down changes in cognitive states that result in dynamic adjustments in

cognitive control. These results also showcase how the model captures post-inhibitory effects

(Rieger & Gauggel, 1999) by adaptive or maladaptive modulation of the proactive inhibitory

channels.

Belief Updating processes driving proactive states

The proactive slowing of the go process is based on dynamically updated beliefs about

prospective SSDs, which are based on tracking previously experienced SSDs. In PRAD, this

belief updating is governed by the μ (persistence) parameter, where $(1 - \mu)$ can be interpreted as

the rate of decay. For $\mu = 1$, the tracked SSD is equal to the average value of all observed SSDs

up to that trial. As μ decreases, a higher recency bias is introduced, with SSD tracking being

biased towards more recent values. Thus, while the tracked SSD generally follows the mean

experienced values, lower values of μ track weigh recent observation more heavily. **Figure 9A**

illustrates three actual participants with different values of μ, demonstrating how high decay

(low $\mu = 0.85$) enables tracking of the most recent observed values of SSD while low decay

(high $\mu = 0.99$) corresponds to tracking the mean observed values over all past trials, and

intermediate decay ($\mu = 0.93$) values balance between these two extremes. On trials when

participants decide to implement a proactive strategy, the go process is delayed by this tracked

belief about SSDs. **Figure 9B** shows how individual differences in participants' decay rates

biases tracked beliefs towards more recent or mean observed SSDs. Persistence in belief

updating (μ) affected the absolute error between tracked and current stop-signal delays ($r = 0.42$,

$p < 0.0001$), with lower μ values associated with higher recency bias, and more accurate dynamic

SSD tracking, and hence more well-calibrated PDR (**Figure 9C**).

This component of PRAD can be construed as engaging both working memory as well as

metacognitive awareness about what level of decay might be ideal in this task, and how this ties

into dynamic adjustments in cognitive control.

Attentional Modulation of Stopping

Attentional Modulation of Stopping (AMS) emerged as a crucial component of inhibitory control

in the PRAD model. AMS is governed by two key parameters: attention-based adaptivity (γ_1)

and attention length ($\gamma 0$). These parameters modulate the stopping expectancy which in turn

affects the variability of SSRT on a trial-by-trial basis.

We observed that within-individual correlation between the number of trials since a stop signal

has last been encountered (nSSD) and (a) the observed SFR average at each nSSD (95% CI of

correlation coefficient ranging from -0.69 to +0.70), (b) the trial level SSRT (95% CI of

correlation coefficient ranging from -0.89 to +0.90) show a wide range of correlations across

individuals. Across participants, the average stopping expectancy ranged from 0.43 to 0.66 (2.5^{th}

to 97.5^{th} percentile). Across all trials and participants, the stopping expectancy ranged from 0.38

to 0.71 (2.5^{th} to 97.5^{th} percentile). Within individuals, the 95% CI width of stopping expectancy

ranges from 0.0 (no modulation) to 0.68, with an average 95% CI of 0.16. This stopping

expectancy is the implicit expectation about the probability of encountering a stop signal; it is the

initial bias of the stopping drift diffusion process, modulating the baseline reactive stopping

process. The within-individual correlation between SFR and trials since stop signal was last

encountered is correlated positively with the average stopping expectancy ($r = 0.48$, $p <0.0001$)

and weakly negatively ($r = -0.135$, $p <0.0001$) with the variability in stopping expectancy

(measured by coefficient of variability). The absolute value of this within-individual correlation

is correlated weakly with average stopping expectancy ($r = 0.052$, $p <0.0001$) and positively ($r =$

0.30, $p <0.0001$) with the variability in stopping expectancy. These trial-level changes in

stopping expectancy form the basis of the AMS process.

The distribution of SSRT and RT (**Figure 10A**) across the sample revealed substantial individual

differences, with SSRT showing greater between-subject variability ($CV = 0.44$) compared to RT

(average $CV = 0.16$). We found that the log ratio of SSRT/RT (**Figure 10B, SI Table S14**) was

significantly influenced by both stop process drift rate ($\beta = -0.27$, $p < 0.0001$) and threshold ($\beta =$

0.63, $p < 0.0001$), accounting for 74% of the variance in this measure. Linear regression (**SI**

Table S14) reveals that after controlling for stop process drift, response thresholds, and non-

decision time (i.e., the remaining parameters affecting SSRT), the AMS driven stopping

expectancy still has an influence on SSRT ($R^2 = 0.84,\ \beta = -0.21,\ p < 0.0001$).

The variability in stopping expectancy represents the strength of the AMS effect, and the

coefficient of variation of stopping expectancy ranged from 0.005 (2.5$^{\text{th}}$ percentile; weak AMS

effect) to 0.229 (97.5$^{\text{th}}$ percentile; moderate AMS effect). The SSRTCV is positively correlated

with variability in stopping expectancy ($r = 0.55$, $p <0.0001$). Linear regression (**SI Table S14,**

$R^2 = 0.83$) shows that average stopping expectancy ($\beta = 0.36$, $p < 0.0001$) and coefficient of

variation of stopping expectancy ($\beta = 0.55$, $p < 0.0001$) have a significant influence on

SSRTCV even after controlling for the effects of stop process drift rate and stop process decision

threshold.

These findings demonstrate the pervasive influence of attentional modulation on stop process

dynamics across our sample, highlighting its role in explaining individual differences in

inhibitory control performance.

Differential patterns of attentional modulation of stopping

To further quantify the impact of attentional modulation on stop process dynamics across our

sample, we analyzed subgroups based on their attentional modulation parameter (γ_1). Analysis

revealed that 58% of participants showed decreasing attentional control ($\gamma_1 < 0$) as the number of

trials since the last stop signal increased, while 42% showed increasing control ($\gamma_1 > 0$). Here

increasing attentional control refers to increasing bias of the stopping process, which on the

presentation of a stop signal stimulus would result in faster SSRTs.

We found significant differences between these subgroups in several key measures as a function

of the number of trials since the last stop signal (nSSD). Changes in stopping expectancy with

nSSD (**Figure 11A**) showed a divergent trend between subgroups (t(7785) = 839, p < 0.0001),

with the $\gamma_1 > 0$ group maintaining higher expectancy as nSSD increased (average r = 0.96), while

the $\gamma_1 < 0$ group showed decreasing expectancy (average r = -0.97). This translated to significant

differences in the correlation of SSRT **(Figure 11B)** and nSSD between subgroups (t(7785) = -

157, p < 0.0001), and correlation of observed SFR **(Figure 11C)** and nSSD between subgroups

(t(7785) = -52, p < 0.0001), with the $\gamma_1 > 0$ group showing more stable performance, in terms of

reducing SFR with nSSD (average correlation -0.21 vs 0.16). Thus, AMS parameters

significantly influenced patterns of stop-failure rates.

Figure 11D illustrates three actual participants with different values of γ_1. The first, with a

negative value, shows how stopping bias (implicit expectation of a stop signal) reduces with

increasing trials since a stop signal was last encountered (nSSD), leading to a corresponding

increase in SSRT as well as SFR at high nSSD. The second, with γ_1 close to zero, show no

specific trend with nSSD, while the third, with positive γ_1 shows increasing stopping bias, along

with reducing SSRT and SFR with higher nSSD. This behavior would be compatible with an

explanation of stronger sustained attention. **Figure 11E** shows how this generalizes across

participants as the value of γ_1 varies.

These results show that the AMS process has a significant effect on SSRT and variability of

SSRT within individuals, as well as on the divergence of observed patterns of reducing or

increasing stopping capacity as the time since the last stop signal was encountered increases.

Thus, the AMS effect seems to be measuring the capacity for sustained attention and its impact

on inhibitory capabilities.

Mechanism for trigger failures

AMS processes also provided a continuous process explanation for what have previously been

termed trigger failures (R. Doekemeijer et al., 2021; Matzke et al., 2017; Skippen et al., 2019), or

assumed failures to initiate the stopping process **(Figure 11F)**.

The total SSD + SSRT is higher than the 90th percentile individual RT for 14% of stop trials

across individuals (95% CI from 0% to 82%; average 5% for stronger factor 2 and 22% for

weaker factor 2). The AMS mechanism in the PRAD model allowed the distribution of SSRTs to

include significantly higher valued SSRTs on some trials, including SSRTs that were higher than

the typical RTs, especially for participants low on factor 2 (weak reactive inhibition), as seen in

Figure 10B. Such trials, in the absence of the PRAD model, which allows for higher variability

in SSRT, would be difficult to explain and be classified as trigger failures within the traditional

account. Compared to the PRAD model, the control RVM model had significantly lower within-

individual SSRT variability (SD) (t(7784) = -58, p<0.0001; 89% of the individuals had higher

inferred within-individual SD of SSRT across trials in the PRAD compared to RVM). The mean

SSRT SD/CV was 0.04/0.119 in the control model compared to 0.060/0.173 in PRAD.

The model identifies not only participants who are more likely to be identified as having a higher

proportion of trigger failures, but also what type of trials these are more likely to be encountered

on – demonstrating that the inferred trigger failure mechanisms may be exceedingly long SSRTs

that are predicated on low stopping expectancy, which in turn is predicated mostly on decreasing

expectancy with increasing trials since a stop signal was last encountered. This account is

compatible with attentional accounts of trigger failures but provides a strong basis for these

attentional lapses based on continuous variability in the stopping process modulated by AMS.

PDR and AMS uncover district sources of intra-individual variability

PRAD uncovered complex interaction dynamics between proactive and reactive control

mechanisms. **Figure 12** demonstrates the variability in PDR and AMS processes across 4

individuals, illustrating how different combinations of these processes can lead to similar overall

performance but through distinct cognitive mechanisms. **Figure 12** compares inferences from

four actual participants: The first two participants have a high variability in PDRs (row 1),

whereas the latter two have a low variability in PDR states, with participant three having almost

no PDRs, and participant four having a consistently high level of PDRs. This manifests as high

variability in RT in the first two, but low variability of RT in the latter two participants (row 2).

Participants one and four have a high variability in of stopping expectancy based on the AMS

mechanism, whereas participants two and three have a stable stopping expectancy across trials

(row 3), representing minimal attentional modulation. This manifests as highly variable SSRT

for the former two, and low variability in SSRT for the latter (row 4). This illustrates how for

instance, very different underlying behavioral patterns between participants 3 and 4 may result in

similar iSSRT estimates based on traditional parametric methods. It also illustrates how the

presence or absence of a strong proactive components (participant 2 vs 3) can reverse inferences

about SSRT between the PRAD model and traditional parametric estimates. Participants two and

four have very similar SFR and similar model inferred median SSRT, although the source of trial

level variability is very different between these participants.

These illustrative results highlight how the model can dissociate different sources of IIV while

observed summary level behavior may be similar. These results also highlight the importance of

considering the dynamic interplay between different control mechanisms when characterizing

individual differences in inhibitory control.

PDR and AMS as compensatory mechanisms for baseline reactive processes

We ran regression models evaluating the effect of factor 2 scores (representing baseline reactive

inhibitory process), average proactive delayed response times, and the interaction between these

measures, on stop failure rate (SFR). The interaction model is significant ($R^2 = 0.62$, p <

0.0001), with significant influence of factor 2 scores (standardized $\beta = 0.2$, p < 0.0001),

proactive delays (standardized $\beta = -0.51$, p < 0.0001), and interaction (standardized $\beta = -0.37$, p

< 0.0001). This reveals that longer average proactive delays reduce stop failure rates as expected,

but more importantly, the interaction shows that baseline reactive processes show sharp

differences in SFR between low and high basic reactive processes when proactive delayed

responses were low, but these differences were minimal when proactive delayed responses were

high. Thus, proactive delayed responses could compensate for weaker reactive baseline

processes.

Next, we ran a regression model evaluating the effect of factor 2 scores (representing baseline

reactive inhibitory process), average stopping expectancies, and the interaction between these

measures, on stop failure rate. The interaction model is significant ($R^2 = 0.35$, p < 0.0001), with

significant influence of factor 2 scores (standardized $\beta = 0.58$, p < 0.0001), stopping

expectancies (standardized $\beta = -0.15$, p < 0.0001), and interaction (standardized $\beta = -0.10$, p <

0.0001). This reveals that higher stopping expectancies could compensate for weaker reactive

baseline processes.

Dynamic interactions between PDR and AMS

PRAD uncovered complex interaction dynamics between proactive and reactive control

mechanisms. **Figure 13** illustrates how individuals can be grouped based on their PDR and AMS

parameters, revealing four distinct adaptivity profiles. These profiles demonstrate various

compensatory relationships between proactive and reactive control.

Specifically, individuals with $\theta_1 < 0$ and $\gamma_1 > 0$ (25.7%) showed the most adaptive dynamic

regulation of processes affecting inhibitory control. Here, when stopping expectancy decreased

(worsening SSRT), the probability of proactivity increased, showing compensatory proactive

mechanisms that worked towards maintaining performance levels (*compensatory – performance*

in **Figures 13A,B**).

Conversely, individuals with $\theta_1 > 0$ and $\gamma_1 > 0$ (16.8%) showed reduction of proactive probability

when SSRT worsened, indicating maladaptive proactive regulation. Rather than compensating,

both reactive and proactive modulation moved in a cohesive manner towards reducing effort

(*cohesive - effort* in **Figures 13A,B**).

Individuals with $\theta_1 > 0$ and $\gamma_1 < 0$ (21.6%) show reduction of proactive probability when

SSRT improves, compatible with a compensatory mechanism that works towards effort-

reduction by reducing proactivity when reactive control is stronger (*compensatory – effort* in

Figures 13A,B).

Finally, individuals with $\theta_1 < 0$ and $\gamma_1 < 0$ (36%) show an increase in proactive probability

when SSRT improves, compatible with a cohesive internal system that improves both reactive

and proactive processes dynamically, possibly in stronger anticipation of a stop trial, but may not

result in strong compensatory action between proactive and reactive mechanisms (*cohesive –*

performance in **Figures 13A,B**).

Thus, the PRAD model allows inferences about multiple trait-like parameters governing

individual differences in dynamic regulation, which provide a multi-faceted view of adaptivity.

The dissociated PDR and AMS processes identified under PRAD reveal distinct and

complementary sources of within-individual adaptivity.

Nonergodicity in cognitive control processes

Nonergodicity in a behavioral context occurs when statistics of a behavior over time (within-

individual dynamics) do not converge to statistics of the behavior over individuals (between-

individual dynamics) (Fisher, Medaglia, & Jeronimus, 2018). In other words, nonergodic

processes exhibit different inferences when behavioral dynamics are analyzed at the within-

individual level compared to the between-individual level. This distinction is crucial because

within-subjects conclusions are often drawn from between-subjects inferences (Curran & Bauer,

2011). Yet, such generalizations are only valid for ergodic processes (Molenaar, 2004).

PRAD revealed substantial evidence for nonergodic processes in inhibitory control.

Specifically, the model uncovered differences between within-subject and between-subject

correlations for both latent and observed measures **(Figures 14A-D)**, indicating nonergodicity.

For example (**SI Table S15**), we observed opposite patterns of within-subject and between

subjects correlations, in the associations between mean experienced stop-signal delay and stop-

failure rate (average within r = 0.22, between = -0.77), RT and probability of proactive state

(average within r = 0.42, between = -0.05), RT and SSRT (average within r = 0.56, between = -

0.13), stop-failure rate and probability of proactive state (average within r = -0.31, between =

0.06), SSRT and average proactive delay (average within r = 0.01, between = -0.39). These

findings suggest that the interactions among cognitive processes underlying response inhibition

are nonergodic, and that within-individual dynamics cannot be fully captured by between-

individual analyses.

1006

The acknowledgment of nonergodicity calls for dynamic, individualized approaches to analyzing

cognitive data, challenging the conventional reliance on aggregated metrics and static models

(Aristodemou, Rommelse, & Kievit, 2022; Cañigueral et al., 2022; Epstein et al., 2022;

Karalunas, Geurts, Konrad, Bender, & Nigg, 2014; Kofler et al., 2013; Kuntsi, 2014; Ode,

Robinson, & Hanson, 2011; Paraskevopoulou, Coon, Brunner, Miller, & Schalk, 2021; Tamm,

Epstein, & Becker, 2019; Wiecki, Poland, & Frank, 2015; Yamashita et al., 2021). The

implications of these findings are twofold. First, they highlight the importance of considering

individual differences in cognitive dynamics when studying response inhibition and other

cognitive processes. Group-level analyses may not adequately capture the complex, time-

dependent relationships between cognitive processes within individuals. Second, the presence of

nonergodicity along with individual differences in within-subject dynamics suggest that

personalized approaches to understanding and modifying cognitive control deficits may be

necessary. Interventions targeting specific cognitive processes, such as proactive control or

attentional modulation, may have different effects depending on an individual's unique cognitive

dynamics.

1022

1023 **PRAD reduces model and measurement biases**

1024

Systematic compensation for known biases in traditional SSRT

PRAD-inferred SSRT demonstrated systematic compensation for known biases in traditional

SSRT estimates (Bissett, Hagen, et al., 2021; Frederick Verbruggen et al., 2019; Verbruggen et

al., 2013). Comparing model-based median SSRT (mean 340ms, SD 155ms) to non-parametric

integration method SSRT (iSSRT, mean 302ms, SD 135ms) revealed that traditional iSSRT

estimates were lower by 38ms on average (t(7786) = -32.3, p < 0.0001), and showed a smaller

degree of individual differences (SD lower by 20ms) between individuals (F(7786,7786) = 0.76,

p < 0.0001).

1033

Crucially, PRAD SSRT estimates were significantly higher for conditions known to lead to

underestimation of traditional non-parametric iSSRT (**Figure 15A-E; SI Table S16**). These

included participants with higher right skew of RT (F(3,7783) = 21.9, p < 0.0001), larger RT

slowdown (F(3, 7783) = 9.3, p < 0.0001), high stop success rates (F(2,7784) = 76.8, p < 0.0001),

higher go-omission rates (t(7785) = 3.4, p < 0.0001) and those classified as race-model violators

(t(7785) = 28.9, p < 0.0001).

1040

For each of these, participants were split into groups based on the relevant measure, and the

difference between the PRAD model inferred median SSRT and non-parametric integrated SSRT

(iSSRT) was assessed for group differences using ANOVA or t-tests as appropriate. For RT

skewness and RT slowdown, participants were split into four groups (quantiles) based on these

measures. For stop success rates, participants were split into three groups based on stop success

being < =25%, 25%-75% and >=75%. Previous literature has recommended assessing non-

parametric SSRT only when stopping success ranges in the 25%-75% range, with

underestimation reported for high success rates (Frederick Verbruggen et al., 2019; Verbruggen

et al., 2013). For go omission rates, participants were split into two groups based on go-omission

rates being < or > 20%. Previous literature has recommended avoiding non-parametric SSRT

when go-omission rates are high (Frederick Verbruggen et al., 2019; Verbruggen et al., 2013).

For Violators (NDAR classification), participants were split into two groups based on whether

they were classified as violators as per the ABCD NDAR classification, which infers violators as

children who seem to violate traditional assumptions of context independence. Significant group

differences *and* increasing SSRT difference as skewness / slowdown increased (Frederick

Verbruggen et al., 2019; Verbruggen et al., 2013), stop success rates / go-omission rates were

higher, or for violators, were indicative of debiased PRAD SSRT.

1058

We confirmed that the relative quality of PRAD model fit under these conditions remained

stronger compared to control models, thus validating these inferences (**SI Table S16**). PRAD

robustly identifies and characterizes response inhibition even when assumptions of the race

model and context independence are violated, effectively compensating for known, systematic

biases in conventional measures. Thus, PRAD effectively characterizes and rectifies biases

inherent in traditional cognitive control models. This is especially important when investigating

neurodevelopmental disorders and older adults who exhibit diminished performance and greater

variability.

1067

Additionally, PRAD revealed systematic differences in previously unexamined conditions, such

as high RT variability ($F(3,7783) = 9.2$, $p<0.0001$), high RT kurtosis ($F(3,7783) = 25.4$,

$p<0.0001$), high SSRT variability ($F(3,7783) = 116$, $p<0.0001$), and low correlations between

SFR and SSD ($F(3,7783) = 72.6$, $p<0.0001$) (**Figures 15F-I**). This detection of other systematic

patterns of differences from non-parametric methods, while exploratory, is indicative that there

may be other previously unexamined specific patterns of behavior that lead to biases in

traditional non-parametric iSSRT estimates, that can be detected by the PRAD models.

1075

1076 These results demonstrate PRAD's ability to provide more accurate and unbiased SSRT

1077 estimates across a wide range of performance patterns, particularly for individuals who deviate

1078 from typical performance profiles, when context independence is violated, or for behavioral

1079 patterns that are not ideal for non-parametric estimation.

1080

Multiple PRAD mechanisms underlie bias reduction and differentiate behavioral subgroups

Biases in traditionally measured SSRT or the ability of models to explain behavior is linked to

behavioral patterns such as violations of context or stochastic independence, high skew,

variability, or slowdown in RT, extreme patterns of SFR or go-omissions, and sequential

dependencies. We analyzed which PRAD model parameters differentiated behavioral subgroups

related to these behavioral patterns (**Figure 16**), and find that parameters related to proactive

mechanisms (factor 1), basic reactive mechanisms (factor 2), and the go-process show strong

effects sizes in terms of differences between behaviorally defined sub-groups.

1089

Reducing typicality biases and improving explanations of individual differences for atypical

profiles

We examined the model fits and residuals for PRAD and the control RVM model on key

behavioral measures. PRAD provided improved fits (lower absolute residuals) to data compared

to RVM for RT (Cohen's d 0.24), RT SD (Cohen's d 1.04), SFR (Cohen's d 0.85), and

correlation between SFR and SSD (Cohen's d 0.27).

1096

For each measure, we evaluated the mean absolute residuals by population subgroups based on:

(i) family income (based on whether income was lower than or greater than $50k annually), (ii)

age (median split), (iii) whether children demonstrated externalizing behavior (based on CBCL

externalizing t-scores > 64), (iv) cognitive ability (median split using NIH cognitive toolbox

scores), (v) brief problem monitoring assessment (BPM scale > 0), (vi) behavioral inhibition

score (median split using the BIS subscale from BIS/BAS), and (vii) adverse life events (median

split using ALE scores). We then compared these mean absolute residuals between the

nontypical and typical subgroups (lower vs higher cognitive ability, younger vs older children,

lower vs higher family income, higher vs lower externalizing, ALE, BIS, and BPM scores) to

compute a *typicality bias*.

1107

We observed that while for most measures, both PRAD and RVM demonstrated some typicality

bias (relatively better fits for typical vs nontypical subgroups), this bias was lower in the PRAD

model vs RVM across all measures and for all of the seven typicality subgroups tested above (**SI**

Table S17). **Figure 17** and **SI Table S17** show the percentage reductions in these measures of

typicality bias by using PRAD compared to the RVM model. Across these four measures and

seven subgroup comparisons, the percentage reduction ranged from 2%-113% with a mean value

of 47%. Importantly, the PRAD model showed lower mean absolute value of residuals for both

typical and nontypical subgroups compared to RVM across all comparisons (i.e., the PRAD

reduction in typicality bias was because of improvements in fits for atypical groups, not because

of poorer fits for typical groups). This reduction in typicality bias compared to the RVM (which

is essentially a Bayesian implementation of a standard horse-race model with competing go and

stop processes, and random variability in SSRT across trials) demonstrates that the PDR and

AMS additions to the PRAD model allow us to more effectively capture the full spectrum of

heterogeneity present in both typical and non-typical or under-represented developing

populations.

1123

1124

1125   **Relevance to cognitive performance, clinical subgroups, neural mechanisms, and**

1126   **exposomic factors**

1127

1128   *Improved Prediction of Cognitive Performance*

1129   PRAD parameters demonstrated superior predictive power for performance on NIH Toolbox

1130   cognitive tasks (Akshoomoff et al., 2013; Slotkin et al., 2012) compared to traditional SSRT

1131   measures. The NIH-Toolbox (NIH-TB) Cognition Battery subtests were used to measure a

1132   diverse set of cognitive domains, including processing speed, executive function, working

1133 memory, and language. Uncorrected scores for the Fluid Cognition Composite Score,

1134 Crystallized Cognition Composite Score, and Total Cognition Composite Score (Akshoomoff et

1135 al., 2013; Slotkin et al., 2012), as well as individual subscores on the following NIH-TB

1136 Cognition Battery subtests were analyzed: Dimensional Change Card Sort Test (Executive

1137 Function/ Set-Shifting), Picture Vocabulary Test (Language), List Sorting Working Memory

1138 Test (Working Memory), Flanker Inhibitory Control and Attention Test (Executive/Attention),

1139 Pattern Comparison Processing Speed Test (Processing Speed), Oral Reading Recognition Test

1140 (Language)

1141

1142 Using support vector machines (SVM regression model with a Gaussian kernel, to assess the fit

1143 as well as 10-fold cross-validated predictions) to fit the overall NIH cognitive toolbox scores, we

1144 found that adjusted R^2 improved from 6.3% to 27.7% when using PRAD parameters instead of

1145 traditional iSSRT measures (**Figure 18A**). The correlations between actual and fitted values

1146 increased from 0.25 to 0.53 (**Figure 18B**). Cross-validated results confirmed this pattern, with

1147 PRAD parameters maintaining higher predictive power (adjusted R^2 = 15.3%; correlations 0.40)

1148 compared to iSSRT (adjusted R^2 = 4.6%; correlations 0.22) (**Figure 18C-D**).

1149

1150 Similar improvements were observed for individual NIH cognitive toolbox tasks and subscores,

1151 including Flanker Inhibitory Control, Dimensional Change Card Sort, and Pattern Comparison

1152 Processing Speed tasks (**SI Table S18; Figure 18**). These findings suggest that PRAD

1153 parameters capture generalizable aspects of cognitive control that extend beyond the specific

1154 context of the stop-signal task, providing a more comprehensive characterization of individual

1155 differences in cognitive abilities.

1156

The NIH Toolbox is an integral component within the Research Domain Criteria (RDoC)

framework, utilized for assessing a wide range of cognitive functions across various disorders

and developmental stages. This comprehensive toolset enables researchers to bridge cognitive

performance with underlying neural and psychological mechanisms, making the PRAD model's

predictive power particularly valuable. Our analysis that parameters derived from the PRAD

model outperformed traditional SSRT metrics for explaining individual differences in tasks

measuring executive function, attention, processing speed, language, and learning/memory, lend

substantial external validity to the PRAD model. By aligning PRAD with tasks from the NIH

Toolbox, our findings highlight the model's capacity to capture cognitive processes that are

foundational across multiple domains of function and dysfunction. This also sets the stage for

future research aimed at integrating cognitive modeling with clinical diagnostics and therapeutic

interventions, guided by the principles of the RDoC framework.

Clinical Relevance

We examined how key PRAD parameters and traditional SSRT measures differed between

specific clinical subgroups based on CBCL evaluations and all other individuals. Groups were

determined based on a CBCL t-score cutoff of 64, identifying children with attention disorders,

rule-breaking, aggression, depression, ADHD, oppositional disorder, and conduct disorder.

SSRT shows a significant difference (with effect size > 0.2) only for ADHD and conduct

disorder, while the PRAD proactive factor showed significant differences (with effect size > 0.2)

for attention, rule-breaking, aggression, ADHD, and conduct disorder, while PRAD go drift rate

showed differences for all of these subgroups. Effect sizes for the drift rate were the largest,

1179 followed by the proactive factor, and lowest for SSRT (**Figure 19A**). This points towards the

1180 emergence of the PRAD drift rate as a transdiagnostic measure, and PRAD proactive control as a

1181 stronger measure for differentiating externalizing disorders compared to SSRT.

1182

Further, we looked at the mean normalized PRAD parameters values for various clinical

subgroups (attention disorders, rule-breaking, aggression, depression, ADHD, oppositional

disorder, conduct disorder, externalizing, internalizing, somatic, and anxiety disorders) based on

the CBCL, as well as typically developing children (as measured by not having membership to

any of these 11 clinical subgroups). Computing a pairwise distance between the subgroups based

on PRAD parameters yields a hierarchy (**Figure 19B**), with externalizing and internalizing

symptoms and diagnosis clustering together, and reveals some interesting patterns, such as

externalizing subgroups showing a higher level of separation from TD compared to internalizing,

and depression falling somewhere in the middle, slightly distinct from other internalizing

subgroups. Importantly, this tells us that the PRAD identifies aspects within the inhibitory

control task that are relevant to graded differences based on patterns of clinical symptoms.

1194

In addition, the key factors tackled in our work – debiased SSRT measurements for extreme

performers, debiased inferences for non-typical or under-represented subgroups, heterogeneity in

intraindividual variability, and heterogeneity in proactive, top-down, and bottom-up regulatory

processes contributing to modulation of inhibitory control may become even more important in

clinical and neurodiverse populations. The distinction between reliance on proactive versus

reactive control mechanisms, as illuminated by the PRAD model, offers a refined lens through

which maladaptive behaviors and transdiagnostic symptoms can be understood. Individual

differences in these control strategies could account for the wide variability in cognitive

performance and behavioral outcomes observed across and within psychiatric disorders. For

instance, children with ADHD have been shown to have impaired reactive but not proactive

inhibition (Pani et al., 2013; van Hulst et al., 2018). Other studies have also shown that

dysfunctional impulsivity is linked to impairments in reactive but not proactive inhibition

(Castro-Meneses et al., 2015). This understanding holds significant promise for tailoring

interventions to target specific cognitive control deficits, moving towards a more personalized

approach in clinical practice. For example, an overreliance on reactive control and a diminished

capacity for proactive control may contribute to impulsive behaviors and difficulty with goal-

directed planning, which are common features of many psychiatric disorders. By considering

individual differences in these control mechanisms, PRAD can help to elucidate the cognitive

processes that may underlie common symptoms across different diagnostic categories, in line

with the RDoC approach.

1215

Neural Relevance

To further validate PRAD's dissociation of reactive and proactive control mechanisms, we

examined their neural correlates at the single-trial level. We examined within-subject trial-level

relationships between PRAD dynamic parameters and brain fMRI activity. Our analysis focused

on core measures of reactive control (trial-level SSRT) and proactive control (trial-level

probability of proactivity, and proactive delaying). The results revealed distinct neural signatures

corresponding to the dynamics of reactive (SSRT) and proactive (probability of proactivity;

proactive delaying) mechanisms within subjects (**Figure 20 A-C**). Network-level (Shirer, Ryali,

Rykhlevskaia, Menon, & Greicius, 2012) visualization of the within-subjects associations

(**Figure 20 D**) revealed that SSRT showed positive associations in the posterior salience,

precuneus, visuospatial, auditory, and sensorimotor networks (all PFDR < 0.01). Probability of

proactivity showed negative associations in the salience and frontoparietal networks, and positive

associations in the default mode network (all PFDR < 0.01), while proactive delaying showed

predominantly negative associations, notably in the salience and frontoparietal networks (all

PFDR < 0.01), but positive associations in the retrosplenial cortex and parahippocampal gyrus

nodes of the ventral default mode network (PFDR < 0.01). These dissociable neural correlates

provide strong validation for PRAD's separation of reactive and proactive control mechanisms,

supporting the model's neural cognitive architecture. A comprehensive analysis of neural

correlates of the PRAD model parameters and demonstration of non-ergodicity in the

neurocognitive dynamics of inhibitory control using the PRAD model can be found in a separate

paper (Mistry, Branigan, Gao, Cai, & Menon, 2024).

1237

Relevance to capturing exposomic factors

We examined the correlation of key PRAD parameters (factors relating to proactive control and

basic reactive control, and go process drift rate), as well as traditional SSRT measures to

exposomic factors including SES (family income category), ALE (adverse life events), and BPM

(Behavioral problem monitoring based on teacher inputs). **Figure 21** shows how the parameter

values change over 4 quantiles of these exposomic factors, along with the underlying correlation.

PRAD measures, especially go process drift (r 0.1 to 0.21; all $p < 0.0001$) and factor 1 pertaining

to proactive control (r 0.08 to 0.14; all $p < 0.0001$) generally show stronger correlations

compared to SSRT (r 0.03 to 0.1; all $p <= 0.011$). Lower income (0.07 to 0.2; all $p < 0.0001$),

higher adverse life events (0.03 to 0.1; all $p <= 0.011$), and higher teacher reported problems (0.1

to 0.21; all $p < 0.0001$), correspond to lower proactive control, weaker go process drift, weaker

reactive control, and higher SSRT.

1250

1251   Combined with the findings that PRAD reduces typicality bias for subpopulations such as

1252   children from lower income families, children with adverse life events, and behavioral problems,

1253   these findings demonstrate the added value of using our approach when examining the role of

1254   exposomic factors.

1255

1256

1257   **Model Reliability and Sensitivity Analysis**

1258

Reliability of model measurements

Behavioral and traditional SSRT measures from the SST task have previously been shown to

have moderate (ICCs 0.34 to 0.57) levels of reliability (Hedge, Powell, & Sumner, 2018), at least

partially attributed to state-dependence of some aspects of the task. Further, these estimates do

not typically include a measure of reliability for second-order observed effects, such as the level

of within-individual correlations between observed variables and experimental contingencies,

which are expected to be even lower.

1266

1267   We first assessed the reliability in behavioral observations across the two runs of SST, yielding

1268   *behavioral ICCs* of 0.12 (SFR), 0.57 (go-omissions), 0.85 (RT), -0.01 (correlation between SFR

1269   and number of trials since the last stop signal), and 0.10 (correlation between SFR and SSD),

1270   with a mean of 0.33 across these measures.

1271

1272   While our primary results are based on jointly fitting data from two separate runs of the SST

1273   task, we also fit each run separately and assessed the reliability in PRAD measures across the

1274   two runs. *PRAD ICCs* ranged from 0.01 to 0.72, with a mean of 0.34 across the model

1275   parameters (**SI Table S19**). Overall, the reliability of PRAD model parameters was within the

1276   same range as demonstrated by behavioral and observed measures in the task.

1277

We note here that moderate reliability in cognitive tasks like the SST has previously been

attributed to low levels of heterogeneity (the 'reliability paradox') in the context of measured

task behaviors and state-dependence of these measures (Hedge et al., 2018), rather than

measurement noise. This is in line with our results, where the model parameter reliabilities are

similar to the reliabilities of different observed measures. Further, the PRAD parameters related

to basic go and reactive stopping processes, as well as average dynamic measures of proactive

delayed responding (PDR), show higher reliability than the model measured SSRT. Further, the

PRAD measures enable dissociating heterogeneity across multiple dimensions, and PRAD

measures related to PDR and AMS such as baseline proactivity (θ_0, 0.69), error-monitoring

sensitivity (θ_1, 1.21), and attention-based adaptivity (γ_1, 1.29) show higher coefficients of

variation compared to SSRT (0.57), which in turn is higher than observed measures like RT

(0.16) and SFR (0.18).

1290

These results demonstrate that the reliability of model parameters seem to be limited only by the

reliability of task behavior itself, but they provide a more dissociated process perspective of

behavior, providing a more nuanced perspective of heterogeneity and individual differences, as

well as identify which processes may contribute more strongly to state-dependence (e.g. AMS),

without any meaningful loss of reliability when compared to traditional or behavioral measures.

Furthermore, with more data collection efforts focused on large datasets with multiple rounds of

measurement, the variability in state-dependent processes like AMS over multiple occasions may

itself be a potentially relevant diagnostic factor.

1299

Sensitivity analysis

We performed a comprehensive set of sensitivity analysis, including testing versions of PRAD

that were fully generative (PRAD-g vs discriminative drift rate estimation), models with an

alternate set of priors for non-decision time (PRAD-n), and subsampling participants based on

MCMC sampling patterns. **SITableS19** shows that ICCs between PRAD and PRAD-g

parameters are 0.9-1.0 and **SI Table S20** shows that all key results highlighted in this paper are

robust to these sensitivity analyses. Details can be found in the **Methods** section.

1307

1308   **Conclusion**

We developed and validated a novel computational model of Proactive, Reactive, and

Attentional Dynamics (PRAD), that characterizes latent proactive, reactive, and attentional

components underlying inhibitory control. We leveraged a very large dataset (N > 7,500) of

children ages 9-10 from the NIH ABCD study, which allowed us to probe distinct sources of

response intraindividual variability in ways that were previously not possible. The ABCD study

provides a unique opportunity to investigate cognitive processes at an unprecedented scale, with

a sample size that far exceeds most previous studies in the field. PRAD demonstrates robustness

to violations of context and stochastic independence, as well as extreme patterns of behavior,

both of which are a limitation for most extant models. PRAD model parameters also provide a

nuanced and integrated perspective on the multiple neurocognitive processes that combine to

produce inhibitory control behavior. We delineate specific mechanisms of proactive control and

attention modulation, demonstrating their interaction and ability to compensate for weak reactive

inhibitory control. The strong influence of proactive control processes on behavioral variability

suggests that factors previously attributed to reactive inhibitory control failures may reflect

breakdowns in proactive control. PRAD as a sophisticated, multicomponent, model offers a

dynamic framework for precisely characterizing goal-directed behaviors, meaningfully

delineating individual differences in cognitive control processes and their functional

consequences, and making theoretical advances in our understanding of cognitive control. PRAD

also reduces biases in latent measures, reduces typicality biases, and provides improved fits to a

wider range of populations and behaviors. These advances will be critical for examining dynamic

neurocognitive mechanisms of inhibitory control in diverse populations.

1330

We have also shown the relevance of PRAD measures to explain individual differences in

performance across a range of executive function, attention, processing speed, language, and

learning/memory tasks compared to conventional models, to understand and dissociate the neural

dynamics underlying proactive and reactive control mechanisms, to identifying differences in

clinical subgroups, and to identifying associations between exposomic factors and differences in

cognitive control processes. By leveraging computational models like PRAD, we anticipate

advancing our understanding of the mechanistic accounts of cognitive disruptions associated

with psychopathology. PRAD's process specificity and explanatory power highlight its potential

for elucidating control deficits in psychopathology and informing individualized interventions.

The availability of dynamic trial-level latent cognitive parameters allows for holistic

investigation of nonergodic neural processes involved in inhibitory control, supporting the RDoC

framework.

1343

1344 More broadly, PRAD exemplifies the utility of sophisticated computational approaches in

1345 unraveling the complex dynamics of cognition. It paves the way for developing models that can

1346 better capture heterogeneity in cognitive processes across populations and advancing our

1347 understanding of mechanisms underlying adaptive and maladaptive behavior.

1348

1350

Participants and inclusion criteria

The present study used a sample of N = 7787 from the Adolescent Brain Cognitive Development

(ABCD) study. The ABCD study is an ongoing, longitudinal study within the United States that

follows a nationally representative sample of children aged 9–10 at baseline (B. J. Casey et al.,

2018; Garavan et al., 2018). Data were from the baseline visit of the ABCD study (Volkow et al.,

2018) (Collection #2573). We report how we determined our sample size, all data exclusions,

and all measures in the study. 9355 participants had two complete runs of the SST task and had

data that were successfully fit with the PRAD model, including checks for convergence. We then

excluded participants who had a glitch reported in the task presentation (N = 257) and those who

had left vs right choice accuracies less than chance level (N = 164). Then, we excluded siblings

by randomly keeping one member from each family (using the genetic_paired_subjectid

variables from gen_y_pihat; $N = 1147$ excluded). Applying these inclusion criteria left us with

a sample of $N = 7787$. See **SI Table S21** for participant demographics.

1364

Stop-Signal Task

Participants completed the SST (Logan, Schachar, & Tannock, 1997) task during fMRI

acquisition. Left and right facing arrows were presented serially as "go" stimuli. Participants

indicated the direction of the arrows using a button box and were instructed to respond as quickly

and accurately as possible, but to withhold their response on a small subset of trials ("stop"

trials) when they saw an upward facing arrow (the "stop" signal), which only appeared after a

brief delay (stop signal delay – SSD). Participants completed two runs of 180 trials each, with

each run including 30 "stop" trials and 150 "go" trials. On stop trials, the time delay between the

"go" and "stop" signals (SSD) was dynamically adjusted by 50 milliseconds increments –

increasing after successful stopping and decreasing after unsuccessful stopping, targeted to

modulate the difficulty levels so that each participant would be able to successfully inhibit their

responses approximately 50% of the time.

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1378

1379 *Estimating behavioral patterns*

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1381 **Violations of stochastic independence.** Based on simulations (Band et al., 2003), a slope of 3.5

1382 corresponds to estimated correlation of 0.2 between RT and SSRT, and we use this benchmark.

1383

1384 **High skew.** benchmarked by inferring the mean / SD of the exponential component of an ex-

1385 Gaussian distribution fit to reaction times, being greater than 150ms (F. Verbruggen et al., 2019).

1386

1387 **High slowdown.** benchmarked by fitting a linear slope of RT over trials that results in RT

1388 increasing by more than 50% from the first to last trials, or a slowing factor of 1.5 (Verbruggen

1389 et al., 2013).

1390

1391 **High RT variability.** This was measured by first inferring the SD of the Gaussian component of

1392 an ex-Gaussian distribution fit to reaction times. Then this measure of SD across all participants

1393 was fit to a mixture of two Gaussian distributions, and high variability was identified as

1394 participants with SD higher than the mean of the larger of the two mixture distributions.

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Computational Modeling – additional details

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Hierarchical Bayesian implementation. The following MCMC sampling hyperparameters were used: Total 4 chains with 30000 samples each. For each chain, we had a burn-in of 10000 samples, and a thinning factor of 10 was used to record 2000 of the remaining 20000 samples, based on which final inferences were made. The Bayesian priors used in the model are described in **SI Table S22**. Convergence was assessed using R-hat <= 1.1 across all chains. For some participants where convergence across 4 chains was difficult to achieve, we assessed and used only convergent samples based on whether 3 or 2 chains converged. Model inferences for 4195 participants (54%) included convergent samples based on 4 chains, for 2409 (31%) included convergent samples based on 3 chains, and for 1183 (15%) included convergent samples based on 2 chains. To ensure that sampling hyperparameters did not have an effect on the results, we ran a sensitivity analysis (**SI Table S20**) to ensure that all major results replicate, when considering only participants based on selective sampling hyperparameters (convergent samples based on 4 chains; convergent samples based on 3 or more chains). For model fitting, reaction-times less than 0.05s and greater than 1s (the experimental response window) were censored.

1413

Parameter Recovery

Additional analysis demonstrated that the model shows strong parameter recovery (**SI Figure S1**). To test parameter recovery, we sampled 750 combinations of parameters inferred from actual data, then generated new simulated data (RT, stopping success, choice accuracy, at a trial

level) using the PRAD model and these combinations of parameters. Finally, we fit this

simulated data using the PRAD model and compared the inferred parameters (recovered) to the

parameters used to simulate the data. Parameter recovery is not an assessment of the validity of

the PRAD model or its assumptions, nor a measure of effectiveness of the Bayesian methods

used to make inferences. It does provide a way to check the implementation of the model,

diagnose any potential identifiability issues (Matzke, Logan, & Heathcote, 2020b), and

understand the adequacy of the ABCD SST experimental designs for making useful model

inferences.

1426

Sensitivity analysis - PRAD-n model. Note that τ_G is a fixed component of non-decision time,

and not strictly comparable to non-decision times in standard DDM models. The priors on τ_G in

the primary analysis are bounded at 0.1s, smaller than typically assumed for parameters that

represent the full non-decision time. For 47% of the participants, the shortest RT is less than

0.1s, so this upper bound would not make an impact ($\tau_G <$ shortest RT) for these participants.

The posterior mean and median inferred values of τ_G are 0.05s. Recent modeling of the SST

process (Weigard et al., 2023), which does *not* consider a separation of non-decision time into

fixed and strategic proactive components found overall mean non-decision time of 0.137s in a

similar sample. Our selected priors for a partial component of this are thus in line with previous

observations. This choice of priors also results in reliable parameter recovery. To ensure that our

results are not dependent on this choice of priors for non-decision time, we ran a sensitivity

analysis allowing the upper bound on the fixed component τ_G of non-decision time to extend up

to 0.3s (**SI Table S20,** NDT prior), which shows that all major results replicate regardless of this

choice of prior.

1441

Sensitivity analysis - PRAD-g model. In the PRAD model, the dynamic drift rate on each trial

depends on the duration of the go stimulus ($stim_t$). On go trials, since this is confounded with

the go RT, it can be argued that this formulation is discriminative rather than a strictly generative

model. To test the robustness of PRAD, we also test a fully generative model (PRAD-g) where

the dynamic drift rate is only applied on stop trials (where the duration of go stimulus is censored

by the onset of the stop signal) and $stim_t$ is not confounded with RT. On go trials, it is retained

as $\delta_0 \, \mathbb{S}_{LR,t}$, similar to previous work (Weigard et al., 2023). **SI Table S20** (PRAD-g) shows that

all major results replicate for this model.

1450

Control Models – RVM. Random variability model is a simplification of the PRAD model

without the dynamic hierarchical components and is equivalent to a full Bayesian

implementation of the traditional horse-race model(Band et al., 2003), but with the addition of

allowing SSRT to vary randomly across trials, based on the parameters of a stopping drift

diffusion process. It can be considered a nested version of PRAD with the following constraints

applied, plus a change in some priors (**SI table S22**): Constraints: $\alpha_{G1} = \alpha_{G2}$, $\delta_{G,t} = \delta_0 \, \mathbb{S}_{LR,t}$,

$\lambda_t = 0, \rho_t = 0, \beta_{S,t} = 0.5$.

1458

1459   **Control Models – FSM:** Fixed SSRT model is a further simplification of RVM, where the

1460   stopping process is not explicitly modeled, but a constant SSRT value is inferred for each

1461   individual which applies to all trials.

1462

1463   *Statistical Testing*

1464 Unless stated otherwise, correlations refer to Pearson's linear correlation coefficient, p-values are

1465 based on two-tailed tests.

1466

A note on effect sizes. To put some of the effect sizes in this paper in context, note that at our

sample size > 7000, there are considerable differences between coefficients of 0.02, 0.05, 0.1, or

0.2. Using random conclusions estimators (Davis-Stober, Dana, Kellen, McMullin, & Bonifay,

2024) the ratio of MSE of a random conclusions estimator to that using the estimator in question

with effect sizes of 0.02, 0.05, 0.1, and 0.2 at a sample size of N ~ 7000 would correspond to

ratios obtained from effect sizes of 0.17, 0.42, 0.84, and 1.67 using a sample size ~ 100.

1473

Factor Analysis. Factor analysis was carried out using the lavaan(Rosseel, 2012) package in

R(Team, 2020) with the following choice of SEM (structural equation model) hyperparameters:

(rotation = "oblimin", estimator = "ML", likelihood = "normal", auto.var = TRUE, auto.efa =

TRUE). To compare and evaluate the adequacy of factor analysis models, we used the following

criteria: CFI (comparative fit index; threshold 0.95), TLI (Tucker-Lewis index; threshold 0.95),

and RMSEA (threshold < 0.08).

1480

1481 *Software*

1482 Data were processed and analyzed using R (Team, 2020), MATLAB, and JAGS (Plummer,

1483 2003) (version 4.3.0).

1484

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1490

1491 **Competing interests**

1492 Authors declare that they have no competing interests.

1493

Data availability

Data used in the preparation of this article were obtained from the Adolescent Brain Cognitive

Development^{SM} (ABCD) Study (https://abcdstudy.org), held in the NIMH Data Archive (NDA).

This is a multisite, longitudinal study designed to recruit more than 10,000 children age 9-10 and

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listing of the study investigators can be found at https://abcdstudy.org/consortium_members/.

ABCD consortium investigators designed and implemented the study and/or provided data but

did not necessarily participate in the analysis or writing of this report. This manuscript reflects

the views of the authors and may not reflect the opinions or views of the NIH or ABCD

consortium investigators.

These data are publicly shared with eligible researchers.

1512

1513   **Code availability**

1514   All code used in this study will be made available upon publication (https://github.com/scsnl).

1515

1516   **Preregistration**

1517   This study was not preregistered.

1518
1519

References

Adams, N. C., & Jarrold, C. (2012). Inhibition in autism: Children with autism have difficulty inhibiting irrelevant distractors but not prepotent responses. *Journal of autism and developmental disorders, 42*(6), 1052-1063.

Akshoomoff, N., Beaumont, J. L., Bauer, P. J., Dikmen, S. S., Gershon, R. C., Mungas, D., . . . Zelazo, P. D. (2013). VIII. NIH Toolbox Cognition Battery (CB): composite scores of crystallized, fluid, and overall cognition. *Monographs of the Society for Research in Child Development, 78*(4), 119-132.

Alderson, R. M., Rapport, M. D., & Kofler, M. J. (2007). Attention-deficit/hyperactivity disorder and behavioral inhibition: a meta-analytic review of the stop-signal paradigm. *Journal of abnormal child psychology, 35*(5), 745-758.

Aristodemou, M., Rommelse, N., & Kievit, R. (2022). Attentiveness modulates reaction-time variability: findings from a population-based sample of 1032 children.

Aron, A. R. (2011). From reactive to proactive and selective control: developing a richer model for stopping inappropriate responses. *Biological psychiatry, 69*(12), e55-e68.

Aron, A. R. (2011). From reactive to proactive and selective control: developing a richer model for stopping inappropriate responses. *Biol Psychiatry, 69*(12), e55-68. doi:10.1016/j.biopsych.2010.07.024

Band, G. P., Van Der Molen, M. W., & Logan, G. D. (2003). Horse-race model simulations of the stop-signal procedure. *Acta psychologica, 112*(2), 105-142.

Bari, A., Mar, A. C., Theobald, D. E., Elands, S. A., Oganya, K. C., Eagle, D. M., & Robbins, T. W. (2011). Prefrontal and monoaminergic contributions to stop-signal task performance in rats. *Journal of Neuroscience, 31*(25), 9254-9263.

Barnes, J. J., Dean, A. J., Nandam, L. S., O'Connell, R. G., & Bellgrove, M. A. (2011). The molecular genetics of executive function: role of monoamine system genes. *Biological psychiatry, 69*(12), e127-e143.

Bissett, P. G. (2014). *Evaluating the independent race model for the stop signal paradigm: Context independence is violated at short stop signal delays*: Vanderbilt University.

Bissett, P. G., Hagen, M. P., Jones, H. M., & Poldrack, R. A. (2021). Design issues and solutions for stop-signal data from the Adolescent Brain Cognitive Development (ABCD) study. *Elife, 10*, e60185.

Bissett, P. G., Jones, H. M., Poldrack, R. A., & Logan, G. D. (2021). Severe violations of independence in response inhibition tasks. *Science advances, 7*(12), eabf4355.

Bonham, M. D., Shanley, D. C., Waters, A. M., & Elvin, O. M. (2021). Inhibitory control deficits in children with oppositional defiant disorder and conduct disorder compared to attention deficit/hyperactivity disorder: A systematic review and meta-analysis. *Research on Child and Adolescent Psychopathology, 49*(1), 39-62.

Braver, T. S. (2012). The variable nature of cognitive control: a dual mechanisms framework. *Trends Cogn Sci, 16*(2), 106-113. doi:10.1016/j.tics.2011.12.010

Braver, T. S., Paxton, J. L., Locke, H. S., & Barch, D. M. (2009). Flexible neural mechanisms of cognitive control within human prefrontal cortex. *Proceedings of the National Academy of Sciences, 106*(18), 7351-7356.

Caglayan, A., Stumpenhorst, K., & Winter, Y. (2021). The Stop Signal Task for Measuring
Behavioral Inhibition in Mice With Increased Sensitivity and High-Throughput
Operation. *Frontiers in behavioral neuroscience, 15*, 777767.
Cai, W., Chen, T., Ide, J. S., Li, C.-S. R., & Menon, V. (2017). Dissociable fronto-operculum-
insula control signals for anticipation and detection of inhibitory sensory cue. *Cerebral*
cortex, 27(8), 4073-4082.
Cai, W., Chen, T., Ryali, S., Kochalka, J., Li, C.-S. R., & Menon, V. (2016). Causal interactions
within a frontal-cingulate-parietal network during cognitive control: Convergent evidence
from a multisite–multitask investigation. *Cerebral cortex, 26*(5), 2140-2153.
Cai, W., Duberg, K., Padmanabhan, A., Rehert, R., Bradley, T., Carrion, V., & Menon, V.
(2019). Hyperdirect insula-basal-ganglia pathway and adult-like maturity of global brain
responses predict inhibitory control in children. *Nature communications, 10*(1), 4798.
Cai, W., George, J. S., Verbruggen, F., Chambers, C. D., & Aron, A. R. (2012). The role of the
right presupplementary motor area in stopping action: two studies with event-related
transcranial magnetic stimulation. *Journal of neurophysiology, 108*(2), 380-389.
Cai, W., Mizuno, Y., Tomoda, A., & Menon, V. (2023). Bayesian dynamical system analysis of
the effects of methylphenidate in children with attention-deficit/hyperactivity disorder: a
randomized trial. *Neuropsychopharmacology, 48*(11), 1690-1698. doi:10.1038/s41386-
023-01668-3
Cai, W., Oldenkamp, C. L., & Aron, A. R. (2011). A proactive mechanism for selective
suppression of response tendencies. *J Neurosci, 31*(16), 5965-5969.
doi:10.1523/JNEUROSCI.6292-10.2011
Cai, W., Warren, S. L., Duberg, K., Yu, A., Hinshaw, S. P., & Menon, V. (2023). Both reactive
and proactive control are deficient in children with ADHD and predictive of clinical
symptoms. *Translational psychiatry, 13*(1), 179.
Cañigueral, R., Ganesan, K., Smid, C. R., Thompson, A., Dosenbach, N. U., & Steinbeis, N.
(2022). Adaptiveness of fluctuations in intra-individual variability of performance is
process-dependent in middle childhood.
Carver, A., Livesey, D., & Charles, M. (2001). Age related changes in inhibitory control as
measured by stop signal task performance. *International Journal of Neuroscience, 107*(1-
2), 43-61.
Casey, B., Cannonier, T., Conley, M. I., Cohen, A. O., Barch, D. M., Heitzeg, M. M., . . .
Garavan, H. (2018). The adolescent brain cognitive development (ABCD) study: imaging
acquisition across 21 sites. *Developmental cognitive neuroscience, 32*, 43-54.
Casey, B. J., Cannonier, T., Conley, M. I., Cohen, A. O., Barch, D. M., Heitzeg, M. M., . . .
Garavan, H. (2018). The adolescent brain cognitive development (ABCD) study: imaging
acquisition across 21 sites. *Developmental cognitive neuroscience, 32*, 43-54.
Casey, B. J., Tottenham, N., Liston, C., & Durston, S. (2005). Imaging the developing brain:
what have we learned about cognitive development? *Trends in cognitive sciences, 9*(3),
104-110.
Castro-Meneses, L. J., Johnson, B. W., & Sowman, P. F. (2015). The effects of impulsivity and
proactive inhibition on reactive inhibition and the go process: insights from vocal and
manual stop signal tasks. *Frontiers in Human Neuroscience, 9*, 529.
Chikazoe, J., Jimura, K., Hirose, S., Yamashita, K.-i., Miyashita, Y., & Konishi, S. (2009).
Preparation to inhibit a response complements response inhibition during performance of
a stop-signal task. *Journal of Neuroscience, 29*(50), 15870-15877.

Covassin, N., de Zambotti, M., Sarlo, M., Tona, G. D. M., Sarasso, S., & Stegagno, L. (2011).
Cognitive performance and cardiovascular markers of hyperarousal in primary insomnia.
International Journal of Psychophysiology, 80(1), 79-86.
Curran, P. J., & Bauer, D. J. (2011). The disaggregation of within-person and between-person
effects in longitudinal models of change. *Annual review of psychology, 62*(1), 583-619.
Davis-Stober, C. P., Dana, J., Kellen, D., McMullin, S. D., & Bonifay, W. (2024). Better
accuracy for better science... through random conclusions. *Perspectives on Psychological*
Science, 19(1), 223-243.
De Weerdt, F., Desoete, A., & Roeyers, H. (2013). Behavioral inhibition in children with
learning disabilities. *Research in developmental disabilities, 34*(6), 1998-2007.
Doekemeijer, R., Verbruggen, F., & Boehler, C. (2021). Face the (trigger) failure: Trigger
failures strongly drive the effect of reward on response inhibition. *Cortex, 139*, 166-177.
Doekemeijer, R. A., Dewulf, A., Verbruggen, F., & Boehler, C. N. (2023). Proactively adjusting
stopping: response inhibition is faster when stopping occurs frequently. *Journal of*
cognition, 6(1).
Eagle, D. M., Lehmann, O., Theobald, D. E., Pena, Y., Zakaria, R., Ghosh, R., . . . Robbins, T.
W. (2009). Serotonin depletion impairs waiting but not stop-signal reaction time in rats:
implications for theories of the role of 5-HT in behavioral inhibition.
Neuropsychopharmacology, 34(5), 1311-1321.
Elchlepp, H., Lavric, A., Chambers, C. D., & Verbruggen, F. (2016). Proactive inhibitory
control: A general biasing account. *Cognitive psychology, 86*, 27-61.
Epstein, J. N., Karalunas, S. L., Tamm, L., Dudley, J. A., Lynch, J. D., Altaye, M., . . . Atluri, G.
(2022). Examining reaction time variability on the stop-signal task in the ABCD study.
Journal of the International Neuropsychological Society, 1-11.
Fisher, A. J., Medaglia, J. D., & Jeronimus, B. F. (2018). Lack of group-to-individual
generalizability is a threat to human subjects research. *Proceedings of the National*
Academy of Sciences, 115(27), E6106-E6115.
Fiterman, O., & Raz, S. (2019). Cognitive, neural and endocrine functioning during late
pregnancy: An Event-Related Potentials study. *Hormones and behavior, 116*, 104575.
Garavan, H., Bartsch, H., Conway, K., Decastro, A., Goldstein, R., Heeringa, S., . . . Zahs, D.
(2018). Recruiting the ABCD sample: Design considerations and procedures.
Developmental cognitive neuroscience, 32, 16-22.
Geurts, H. M., van den Bergh, S. F., & Ruzzano, L. (2014). Prepotent response inhibition and
interference control in autism spectrum disorders: Two meta-analyses. *Autism Research,*
7(4), 407-420.
Ghasemian, S., Vardanjani, M. M., Sheibani, V., & Mansouri, F. A. (2021). Dimensional bias
and adaptive adjustments in inhibitory control of monkeys. *Animal Cognition, 24*(4), 815-
828.
Godlove, D. C., Emeric, E. E., Segovis, C. M., Young, M. S., Schall, J. D., & Woodman, G. F.
(2011). Event-related potentials elicited by errors during the stop-signal task. I. Macaque
monkeys. *Journal of Neuroscience, 31*(44), 15640-15649.
Hall, J. R., Bernat, E. M., & Patrick, C. J. (2007). Externalizing psychopathology and the error-
related negativity. *Psychological science, 18*(4), 326-333.
Heathcote, A., & Love, J. (2012). Linear deterministic accumulator models of simple choice.
Frontiers in psychology, 3, 292.

Hedge, C., Powell, G., & Sumner, P. (2018). The reliability paradox: Why robust cognitive tasks
do not produce reliable individual differences. *Behavior research methods, 50*(3), 1166-
1186.
Hsu, H. M., & Hsieh, S. (2022). Age-related post-error slowing and stimulus repetition effect in
motor inhibition during a stop-signal task. *Psychological research, 86*(4), 1108-1121.
Hu, S., & Li, C. S. R. (2012). Neural processes of preparatory control for stop signal inhibition.
Human brain mapping, 33(12), 2785-2796.
Ide, J. S., Shenoy, P., Angela, J. Y., & Chiang-Shan, R. L. (2013). Bayesian prediction and
evaluation in the anterior cingulate cortex. *Journal of Neuroscience, 33*(5), 2039-2047.
Ivanov, I., Schulz, K. P., London, E. D., & Newcorn, J. H. (2008). Inhibitory control deficits in
childhood and risk for substance use disorders: a review. *The American journal of drug
and alcohol abuse, 34*(3), 239-258.
Jahfari, S., Stinear, C. M., Claffey, M., Verbruggen, F., & Aron, A. R. (2010). Responding with
restraint: what are the neurocognitive mechanisms? *Journal of cognitive neuroscience,
22*(7), 1479-1492.
Kalanthroff, E., Teichert, T., Wheaton, M. G., Kimeldorf, M. B., Linkovski, O., Ahmari, S. E., . .
. Simpson, H. B. (2017). The role of response inhibition in medicated and unmedicated
obsessive-compulsive disorder patients: evidence from the stop-signal task. *Depression
and Anxiety, 34*(3), 301-306.
Karalunas, S. L., Geurts, H. M., Konrad, K., Bender, S., & Nigg, J. T. (2014). Annual research
review: Reaction time variability in ADHD and autism spectrum disorders: Measurement
and mechanisms of a proposed trans-diagnostic phenotype. *Journal of Child Psychology
and Psychiatry, 55*(6), 685-710.
Kofler, M. J., Rapport, M. D., Sarver, D. E., Raiker, J. S., Orban, S. A., Friedman, L. M., &
Kolomeyer, E. G. (2013). Reaction time variability in ADHD: a meta-analytic review of
319 studies. *Clinical psychology review, 33*(6), 795-811.
Korenblum, C. B., Chen, S. X., Manassis, K., & Schachar, R. J. (2007). Performance monitoring
and response inhibition in anxiety disorders with and without comorbid ADHD.
Depression and Anxiety, 24(4), 227-232.
Kuntsi, J. (2014). Commentary: From noise to insight? Reaction time variability in ADHD and
autism spectrum disorders–a commentary on Karalunas et al.(2014). *Journal of Child
Psychology and Psychiatry, 55*(6), 711-713.
Lavagnino, L., Arnone, D., Cao, B., Soares, J. C., & Selvaraj, S. (2016). Inhibitory control in
obesity and binge eating disorder: A systematic review and meta-analysis of
neurocognitive and neuroimaging studies. *Neuroscience & Biobehavioral Reviews, 68*,
714-726.
Lee, W.-T., & Kang, M.-S. (2020). Electrophysiological evidence for distinct proactive control
mechanisms in a stop-signal task: an individual differences approach. *Frontiers in
psychology, 11*, 1105.
Li, C.-s. R., Huang, C., Yan, P., Bhagwagar, Z., Milivojevic, V., & Sinha, R. (2008). Neural
correlates of impulse control during stop signal inhibition in cocaine-dependent men.
Neuropsychopharmacology, 33(8), 1798-1806.
Li, C.-s. R., Milivojevic, V., Kemp, K., Hong, K., & Sinha, R. (2006). Performance monitoring
and stop signal inhibition in abstinent patients with cocaine dependence. *Drug and
alcohol dependence, 85*(3), 205-212.

Li, F.-F., Chen, X.-l., Zhang, Y.-t., Li, R.-t., & Li, X. (2021). The role of prepotent response inhibition and interference control in depression. *Cognitive Neuropsychiatry, 26*(6), 441-454.

Lipszyc, J., & Schachar, R. (2010). Inhibitory control and psychopathology: a meta-analysis of studies using the stop signal task. *Journal of the International Neuropsychological Society, 16*(6), 1064-1076.

Liu, S., Heitz, R. P., & Bradberry, C. W. (2009). A touch screen based stop signal response task in rhesus monkeys for studying impulsivity associated with chronic cocaine self-administration. *Journal of neuroscience methods, 177*(1), 67-72.

Logan, G. D., & Cowan, W. B. (1984). On the ability to inhibit thought and action: A theory of an act of control. *Psychological review, 91*(3), 295.

Logan, G. D., Schachar, R. J., & Tannock, R. (1997). Impulsivity and inhibitory control. *Psychological science, 8*(1), 60-64.

Logan, G. D., Van Zandt, T., Verbruggen, F., & Wagenmakers, E.-J. (2014). On the ability to inhibit thought and action: general and special theories of an act of control. *Psychological review, 121*(1), 66.

Ma, N., & Yu, A. J. (2015). Statistical learning and adaptive decision-making underlie human response time variability in inhibitory control. *Frontiers in psychology, 6*, 1046.

Matzke, D., Logan, G. D., & Heathcote, A. (2020a). A cautionary note on evidence-accumulation models of response inhibition in the stop-signal paradigm. *Computational Brain & Behavior, 3*(3), 269-288.

Matzke, D., Logan, G. D., & Heathcote, A. (2020b). A cautionary note on evidence-accumulation models of response inhibition in the stop-signal paradigm. *Computational Brain & Behavior, 3*, 269-288.

Matzke, D., Love, J., & Heathcote, A. (2017). A Bayesian approach for estimating the probability of trigger failures in the stop-signal paradigm. *Behavior research methods, 49*, 267-281.

Matzke, D., Love, J., Wiecki, T. V., Brown, S. D., Logan, G. D., & Wagenmakers, E.-J. (2013). Release the BEESTS: Bayesian estimation of ex-Gaussian stop-signal reaction time distributions. *Frontiers in psychology, 4*, 918.

Mayse, J. D., Nelson, G. M., Park, P., Gallagher, M., & Lin, S.-C. (2014). Proactive and reactive inhibitory control in rats. *Frontiers in neuroscience, 8*, 104.

McTeague, L. M., Huemer, J., Carreon, D. M., Jiang, Y., Eickhoff, S. B., & Etkin, A. (2017). Identification of common neural circuit disruptions in cognitive control across psychiatric disorders. *American Journal of Psychiatry, 174*(7), 676-685.

Menon, V. (2011). Large-scale brain networks and psychopathology: a unifying triple network model. *Trends in cognitive sciences, 15*(10), 483-506.

Menon, V. (2013). Developmental pathways to functional brain networks: emerging principles. *Trends in cognitive sciences, 17*(12), 627-640.

Menon, V., Adleman, N. E., White, C. D., Glover, G. H., & Reiss, A. L. (2001). Error-related brain activation during a Go/NoGo response inhibition task. *Human brain mapping, 12*(3), 131-143.

Mirabella, G. (2023). Beyond Reactive Inhibition: Unpacking the Multifaceted Nature of Motor Inhibition. In (Vol. 13, pp. 804): MDPI.

1744   Mistry, P. K., Branigan, N. K., Gao, Z., Cai, W., & Menon, V. (2024). Nonergodicity and
1745   Simpson's paradox in neurocognitive dynamics of cognitive control. *bioRxiv*, 2024.2007.
1746   2005.602273.
1747   Mistry, P. K., Chang, H., El-Said, D., & Menon, V. (2025). Unraveling latent cognitive,
1748   metacognitive, strategic, and affective processes underlying children's problem-solving
1749   using Bayesian cognitive modeling. *bioRxiv*, 2025.2001. 2029.635409.
1750   Mistry, P. K., Skewes, J., & Lee, M. D. (2018). *An Adaptive Signal Detection Model Applied to*
1751   *Perceptual Learning.* Paper presented at the 40th Annual Meeting of the Cognitive
1752   Science Society: Changing Minds, CogSci 2018.
1753   Mistry, P. K., & Trueblood, J. S. (2015). *Reconstructing the Bayesian Adaptive Toolbox:*
1754   *Challenges of a dynamic environment and partial information acquisition.* Paper
1755   presented at the Proceedings of the 37th Annual Meeting of the Cognitive Science
1756   Society, CogSci 2015.
1757   Molenaar, P. C. (2004). A manifesto on psychology as idiographic science: Bringing the person
1758   back into scientific psychology, this time forever. *Measurement, 2*(4), 201-218.
1759   Moore, T. M., Visoki, E., Argabright, S. T., Didomenico, G. E., Sotelo, I., Wortzel, J. D., . . .
1760   Warrier, V. (2022). Modeling environment through a general exposome factor in two
1761   independent adolescent cohorts. *Exposome, 2*(1), osac010.
1762   Murray, K. T., & Kochanska, G. (2002). Effortful control: Factor structure and relation to
1763   externalizing and internalizing behaviors. *Journal of abnormal child psychology, 30*, 503-
1764   514.
1765   Nigg, J. (2017). On the relations among self-regulation, self-control, executive functioning,
1766   effortful control, cognitive control, impulsivity, risk-taking, and inhibition for
1767   developmental psychopathology. *Journal of Child Psychology and Psychiatry, 58*(4),
1768   361-383.
1769   Ode, S., Robinson, M. D., & Hanson, D. M. (2011). Cognitive-emotional dysfunction among
1770   noisy minds: predictions from individual differences in reaction time variability.
1771   *Cognition and Emotion, 25*(2), 307-327.
1772   Olvet, D. M., & Hajcak, G. (2008). The error-related negativity (ERN) and psychopathology:
1773   Toward an endophenotype. *Clinical psychology review, 28*(8), 1343-1354.
1774   Oosterlaan, J., & Sergeant, J. A. (1996). Inhibition in ADHD, aggressive, and anxious children:
1775   A biologically based model of child psychopathology. *Journal of abnormal child*
1776   *psychology, 24*, 19-36.
1777   Pani, P., Menghini, D., Napolitano, C., Calcagni, M., Armando, M., Sergeant, J., & Vicari, S.
1778   (2013). Proactive and reactive control of movement are differently affected in attention
1779   deficit hyperactivity disorder children. *Research in developmental disabilities, 34*(10),
1780   3104-3111.
1781   Paraskevopoulou, S. E., Coon, W. G., Brunner, P., Miller, K. J., & Schalk, G. (2021). Within-
1782   subject reaction time variability: Role of cortical networks and underlying
1783   neurophysiological mechanisms. *Neuroimage, 237*, 118127.
1784   Perri, R. L. (2020). Is there a proactive and a reactive mechanism of inhibition? Towards an
1785   executive account of the attentional inhibitory control model. *Behavioural brain*
1786   *research, 377*, 112243.
1787   Plummer, M. (2003). *JAGS: A program for analysis of Bayesian graphical models using Gibbs*
1788   *sampling.* Paper presented at the Proceedings of the 3rd international workshop on
1789   distributed statistical computing.

Rieger, M., & Gauggel, S. (1999). Inhibitory after-effects in the stop signal paradigm. *British Journal of Psychology, 90*(4), 509-518.

Rosseel, Y. (2012). lavaan: An R package for structural equation modeling. *Journal of statistical software, 48*, 1-36.

Sarkar, S., Choudhury, S., Islam, N., Chowdhury, M. S. J. H., Chowdhury, M. T. I., Baker, M. R., . . . Kumar, H. (2020). Effects of diazepam on reaction times to stop and go. *Frontiers in human neuroscience, 14*, 567177.

Schachar, R., & Logan, G. D. (1990). Impulsivity and inhibitory control in normal development and childhood psychopathology. *Developmental psychology, 26*(5), 710.

Schachar, R., Tannock, R., Marriott, M., & Logan, G. (1995). Deficient inhibitory control in attention deficit hyperactivity disorder. *Journal of abnormal child psychology, 23*, 411-437.

Schachar, R. J., Chen, S., Logan, G. D., Ornstein, T. J., Crosbie, J., Ickowicz, A., & Pakulak, A. (2004). Evidence for an error monitoring deficit in attention deficit hyperactivity disorder. *Journal of abnormal child psychology, 32*, 285-293.

Schmid, J. M., Labuhn, A. S., & Hasselhorn, M. (2011). Response inhibition and its relationship to phonological processing in children with and without dyslexia. *International Journal of Disability, Development and Education, 58*(1), 19-32.

Schmitt, L. M., White, S. P., Cook, E. H., Sweeney, J. A., & Mosconi, M. W. (2018). Cognitive mechanisms of inhibitory control deficits in autism spectrum disorder. *Journal of Child Psychology and Psychiatry, 59*(5), 586-595.

Schroder, H. S., Nickels, S., Cardenas, E., Breiger, M., Perlo, S., & Pizzagalli, D. A. (2020). Optimizing assessments of post-error slowing: A neurobehavioral investigation of a flanker task. *Psychophysiology, 57*(2), e13473.

Senderecka, M., Grabowska, A., Szewczyk, J., Gerc, K., & Chmylak, R. (2012). Response inhibition of children with ADHD in the stop-signal task: An event-related potential study. *International Journal of Psychophysiology, 85*(1), 93-105.

Shenoy, P., & Yu, A. J. (2011). Rational decision-making in inhibitory control. *Frontiers Human Neuroscience, 5*, 48.

Shirer, W. R., Ryali, S., Rykhlevskaia, E., Menon, V., & Greicius, M. D. (2012). Decoding subject-driven cognitive states with whole-brain connectivity patterns. *Cerebral cortex, 22*(1), 158-165.

Sjoerds, Z., Van Den Brink, W., Beekman, A., Penninx, B., & Veltman, D. (2014). Response inhibition in alcohol-dependent patients and patients with depression/anxiety: a functional magnetic resonance imaging study. *Psychological medicine, 44*(8), 1713-1725.

Skippen, P., Matzke, D., Heathcote, A., Fulham, W. R., Michie, P., & Karayanidis, F. (2019). Reliability of triggering inhibitory process is a better predictor of impulsivity than SSRT. *Acta psychologica, 192*, 104-117.

Slotkin, J., Kallen, M., Griffith, J., Magasi, S., Salsman, J., & Nowinski, C. (2012). NIH toolbox. *Technical Manual.[Google Scholar]*.

Smith, J. L., Mattick, R. P., Jamadar, S. D., & Iredale, J. M. (2014). Deficits in behavioural inhibition in substance abuse and addiction: a meta-analysis. *Drug and alcohol dependence, 145*, 1-33.

Soreni, N., Crosbie, J., Ickowicz, A., & Schachar, R. (2009). Stop signal and conners' continuous performance tasks: Test—retest reliability of two inhibition measures in adhd children. *Journal of Attention Disorders, 13*(2), 137-143.

Svaldi, J., Naumann, E., Trentowska, M., & Schmitz, F. (2014). General and food-specific inhibitory deficits in binge eating disorder. *International Journal of Eating Disorders, 47*(5), 534-542.

Swann, N., Poizner, H., Houser, M., Gould, S., Greenhouse, I., Cai, W., . . . Aron, A. R. (2011). Deep brain stimulation of the subthalamic nucleus alters the cortical profile of response inhibition in the beta frequency band: a scalp EEG study in Parkinson's disease. *Journal of Neuroscience, 31*(15), 5721-5729.

Swann, N. C., Cai, W., Conner, C. R., Pieters, T. A., Claffey, M. P., George, J. S., . . . Tandon, N. (2012). Roles for the pre-supplementary motor area and the right inferior frontal gyrus in stopping action: electrophysiological responses and functional and structural connectivity. *Neuroimage, 59*(3), 2860-2870.

Tamm, L., Epstein, J. N., & Becker, S. P. (2019). A preliminary investigation of reaction time variability in relation to social functioning in children evaluated for ADHD. *Child neuropsychology, 25*(7), 885-898.

Team, R. C. (2020). RA language and environment for statistical computing, R Foundation for Statistical. *Computing*.

Toga, A. W., Thompson, P. M., & Sowell, E. R. (2006). Mapping brain maturation. *Trends in neurosciences, 29*(3), 148-159.

Tsvetanov, K. A., Ye, Z., Hughes, L., Samu, D., Treder, M. S., Wolpe, N., . . . Rowe, J. B. (2018). Activity and connectivity differences underlying inhibitory control across the adult life span. *Journal of Neuroscience, 38*(36), 7887-7900.

van Hulst, B. M., de Zeeuw, P., Vlaskamp, C., Rijks, Y., Zandbelt, B. B., & Durston, S. (2018). Children with ADHD symptoms show deficits in reactive but not proactive inhibition, irrespective of their formal diagnosis. *Psychological medicine, 48*(15), 2515-2521.

Verbruggen, F., Aron, A. R., Band, G. P., Beste, C., Bissett, P. G., Brockett, A. T., . . . Colonius, H. (2019). A consensus guide to capturing the ability to inhibit actions and impulsive behaviors in the stop-signal task. *Elife, 8*, e46323.

Verbruggen, F., Aron, A. R., Band, G. P., Beste, C., Bissett, P. G., Brockett, A. T., . . . Boehler, C. N. (2019). A consensus guide to capturing the ability to inhibit actions and impulsive behaviors in the stop-signal task. *Elife, 8*. doi:10.7554/eLife.46323

Verbruggen, F., Chambers, C. D., & Logan, G. D. (2013). Fictitious inhibitory differences: how skewness and slowing distort the estimation of stopping latencies. *Psychological science, 24*(3), 352-362.

Verbruggen, F., & Logan, G. D. (2008). Response inhibition in the stop-signal paradigm. *Trends in cognitive sciences, 12*(11), 418-424.

Verbruggen, F., & Logan, G. D. (2009a). Models of response inhibition in the stop-signal and stop-change paradigms. *Neuroscience & Biobehavioral Reviews, 33*(5), 647-661.

Verbruggen, F., & Logan, G. D. (2009b). Proactive adjustments of response strategies in the stop-signal paradigm. *Journal of Experimental Psychology: Human Perception and Performance, 35*(3), 835.

Vink, M., Kaldewaij, R., Zandbelt, B. B., Pas, P., & du Plessis, S. (2015). The role of stop-signal probability and expectation in proactive inhibition. *European Journal of Neuroscience, 41*(8), 1086-1094.

Volkow, N. D., Koob, G. F., Croyle, R. T., Bianchi, D. W., Gordon, J. A., Koroshetz, W. J., . . . Weiss, S. R. B. (2018). The conception of the ABCD study: From substance use to a broad NIH collaboration. *Dev Cogn Neurosci, 32*, 4-7. doi:10.1016/j.dcn.2017.10.002

Wabersich, D., & Vandekerckhove, J. (2014). Extending JAGS: A tutorial on adding custom
distributions to JAGS (with a diffusion model example). *Behavior research methods, 46*,
15-28.
Weigard, A., Heathcote, A., Matzke, D., & Huang-Pollock, C. (2019). Cognitive modeling
suggests that attentional failures drive longer stop-signal reaction time estimates in
attention deficit/hyperactivity disorder. *Clinical Psychological Science, 7*(4), 856-872.
Weigard, A., Matzke, D., Tanis, C., & Heathcote, A. (2021a). Cognitive process modeling
addresses context independence violations in the ABCD Study stop-signal task. *bioRxiv*,
2021.2007. 2026.453872.
Weigard, A., Matzke, D., Tanis, C., & Heathcote, A. (2021b). Cognitive process modeling
addresses context independence violations in the ABCD Study stop-signal task. *BioRxiv*.
Weigard, A., Matzke, D., Tanis, C., & Heathcote, A. (2023). A cognitive process modeling
framework for the ABCD study stop-signal task. *Developmental Cognitive Neuroscience,
59*, 101191.
Wessel, J. R., Diesburg, D. A., Chalkley, N. H., & Greenlee, J. D. (2022). A causal role for the
human subthalamic nucleus in non-selective cortico-motor inhibition. *Current biology,
32*(17), 3785-3791. e3783.
Wiecki, T. V., Poland, J., & Frank, M. J. (2015). Model-Based Cognitive Neuroscience
Approaches to Computational Psychiatry. *Clinical Psychological Science, 3*(3), 378-399.
doi:10.1177/2167702614565359
Williams, B. R., Ponesse, J. S., Schachar, R. J., Logan, G. D., & Tannock, R. (1999).
Development of inhibitory control across the life span. *Developmental psychology, 35*(1),
205.
Yamashita, A., Rothlein, D., Kucyi, A., Valera, E. M., Germine, L., Wilmer, J., . . . Esterman, M.
(2021). Variable rather than extreme slow reaction times distinguish brain states during
sustained attention. *Scientific reports, 11*(1), 1-13.
Yu, F., Huang, Y., Chen, T., Wang, X., Guo, Y., Fang, Y., . . . Zhang, L. (2022). Repetitive
transcranial magnetic stimulation promotes response inhibition in patients with major
depression during the stop-signal task. *Journal of Psychiatric Research*.
Zhao, W., Gao, D., Yue, F., Wang, Y., Mao, D., Chen, X., & Lei, X. (2018). Response inhibition
deficits in insomnia disorder: an event-related potential study with the stop-signal task.
Frontiers in Neurology, 9, 610.
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1916 **Figure 1. Overview of the stop signal task and analysis pipeline.** Illustration of Go and Stop
1917 trials in the stop signal task. On Go trials, participants respond to indicate arrow direction; on
1918 Stop trials, they must inhibit their response when the stop signal appears.

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1921   **Figure 2.** Proportion of participants for whom traditional SSRT measure may not be suitable
1922   (green) and for whom models with additional explanatory mechanisms may be required (blue).

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Figure 3. Schematic of the Proactive Reactive and Attentional Dynamics (PRAD) model.
(A) Overview of how latent cognitive processes interact to produce observed behavior. The
model infers latent variables related to three mechanisms of dynamic inhibitory control: basic
reactive inhibition, proactive response delaying, and attentional modulation of stopping
expectancy. **(B)** Mathematical details of the model, showing two drift diffusion processes (go,
stop) augmented with dynamic parameters. Blue - individual-level parameters, Red - trial-level
dynamic parameters.

Figure 4. Model fit comparisons. (A-F) Aggregate behavior patterns for stop-failure rates (SFR) across different stop-signal delays (SSD) and number of trials since last stop signal (nSSD), comparing actual data with predictions from PRAD and control models (RVM and FSM). PRAD uniquely accounts for subgroup differences in SFR-SSD and SFR-nSSD relationships. **(G)** Root mean square error (RMSE) comparisons across models for various behavioral measures, showing PRAD's superior fit. RMSE computed based on the distance between binned aggregate curves (actuals vs model posterior generated values). **(H)** Improvements in individual-level fit correlations using PRAD compared to control models across multiple behavioral measures. Dark green – actuals, Light green – PRAD, dark blue – RVM, light blue – FSM. RVM = Random Variability control model; FSM = Fixed SSRT control model.

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1950 **Figure 5. Illustrative single-participant dynamics on stop trials. (A)** Trial-by-trial
1951 fluctuations in stopping expectancy, SSRT, SSD, PDR, and RT, illustrating the complex
1952 interplay of these variables. **(B)** Comparison of three specific stop trials (16, 19, and 39)
1953 demonstrating how different combinations of SSD, SSRT, and PDR lead to successful stops or
1954 failures, highlighting the model's ability to capture nuanced trial-level dynamics. On stop trial
1955 16, SSD is low (easy trial), but it still results in a stop-failure as there is no proactive delaying of
1956 the go process (PDR ~ 0), and RT < (SSD+SSRT). On stop trial 19, SSD is higher (difficult
1957 trial), but SSRT is much lower because stopping expectancy is higher (attentional modulation of
1958 SSRT), resulting in a successful stop. On stop trial 39, SSD is even higher (very difficult), and
1959 stopping expectancy is not very high, resulting in a high SSRT. However, in spite of SSD+SSRT
1960 being higher than stop trial 16, this trial does not result in a stop-failure because of the influence
1961 of proactive delay of the go process (high PDR).
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1965 **Figure 6. Core components of the PRAD model. (A)** Illustration of three key inhibitory
1966 subprocesses: (1) basic reactive inhibition (red box), where competing Stop and Go processes
1967 determine trial outcome; (2) proactive delayed responding (PDR, green box), where anticipatory
1968 delaying of the Go process can lead to successful stopping; and (3) attentional modulation of
1969 stopping expectancy (yellow box), where top-down modulation can influence SSRT. **(B)** Factor
1970 analysis results showing how seven key PRAD parameters load onto three distinct factors
1971 corresponding to these subprocesses – proactive control, basic reactive control, and attentional
1972 modulation – demonstrating the model's ability to dissociate different aspects of inhibitory
1973 control.

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1976   **Figure 7. Proactive Delayed Response (PDR). (A)** Distribution of median PDR and RT across
1977   individuals, showing the range of proactive control strategies. **(B)** Distribution of average
1978   probability of proactive states across participants.
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1982 **Figure 8. PDR dynamics. (A) Illustration of error monitoring and modulation of proactive**
1983 **states.** Trial-level dynamics (probability of proactivity) from two participants with high negative
1984 (adaptive) and positive (maladaptive) θ_1 values. **(B) Distribution of error monitoring related**
1985 **sequential effects on probability of proactivity.** Distribution of average changes in trial level
1986 probability of proactivity after stop failures versus after go omissions. The colors reflect
1987 θ_1 values. Participants with negative values (red) tend to show more adaptive error-based
1988 modulation while those with positive values (blue) tend to show more maladaptive error-based
1989 modulation of proactivity. **(C)** Differences in post stop-failure proactivity between θ_1 subgroups.
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Figure 9. PDR dynamics. (A) Illustration of belief updating and tracking SSD for proactive delaying. Trial-level dynamics including tracking weights (bar chart), and how noisy tracking of SSD (black lines) is related to last observed (red) and mean observed (blue) SSD, depending on high, medium, or low decay rates for belief updating in the tracking process. Participants with higher decay (low persistence μ) are closer to last observed SSD, while those with lower decay (high persistence μ) are closer to mean observed SSD. **(B, C) Effect of decay rate / persistence on tracking errors.**

Figure 10. Attentional Modulation of Stopping (AMS). (A) Distribution of median SSRT and RT across individuals. **(B) Distribution of the log ratio of SSRT to RT across participants, and link to stopping process parameters.**

Figure 11. Attentional Modulation of Stopping (AMS) dynamics. **(A-C)** Evolution of stopping dynamics (expectancy, SSRT, and SFR) with increasing trials since last stop signal (nSSD) for different attentional modulation subgroups ($\gamma_1 > 0$ vs $\gamma_1 < 0$), showing adaptive and maladaptive patterns. **(D) Illustration of AMS and dynamics of stopping process.** Trial-level dynamics including stopping expectancy or bias (light blue), the resulting SSRT (dark blue), and the subsequently resulting SFR (orange), as a function of n(SSD), the number of trials since a stop signal was last encountered. The participants with different positive and negative values of γ_1 show different patterns of positive and negative change. **(E)** Distribution of how SSRT and SFR are related to n(SSD) across participants, based on the underlying γ_1 values. **(F)** **Explanatory mechanisms for stop 'trigger failures'.** Proportion of stop trials where the SSRT+SSD was higher than the 90th percentile RT (at an individual level), as a function of trial level dynamic stopping expectancy.

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Figure 12. Illustration of variability in PDR and AMS processes across four representative participants. Comparison of trial-by-trial fluctuations in PDR, RT, stopping expectancy, and SSRT, demonstrating how similar overall performance can arise from different underlying cognitive dynamics. This figure highlights how the PRAD model can dissociate different sources of intra-individual variability that may be indistinguishable using traditional measures.

Figure 13. Dynamic interactions between PDR and AMS processes. (A) Four categories of
interactions based on values of γ_1 and θ_1, and the resulting changes in trial level probability of
proactivity when stopping expectancy (bias) increases or decreases. **(B)** Distribution of changes
in trial level probability of proactivity (color coded) when stopping expectancy (bias) increases
(left) or decreases (right), as a function of γ_1 and θ_1.

2044 **Figure 14. Evidence for nonergodicity in cognitive dynamics.** Comparison of within-subject
2045 (green) and between-subject (blue) correlations for various pairs of observed and latent variables.
2046 Differences between these correlations, especially sign changes, indicate nonergodic processes.
2047 Notable nonergodic effects are observed in some of the relationships between mean experienced
2048 SSD, SFR, SSRT, RT, PDR, and probability of proactive state. The between-subjects values
2049 plotted are based on average values for individuals and bootstrapping the sample. SFR: Stop
2050 failure rate, SSRT: Stop-signal reaction time, RT: Reaction time, PDR: Proactive delayed
2051 responding, p_{pro}: probability of proactive cognitive state. Error bars reflect 2.5th to 97.5th
2052 percentiles for within subject correlations and 2.5th to 97.5th percentiles based on bootstrapped
2053 samples for between subject correltions.

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2056 **Figure 15. Debiasing of stop-signal reaction time (SSRT) estimates.** Comparison of PRAD-
2057 inferred SSRT with traditional non-parametric integrated SSRT (iSSRT) across various
2058 conditions. **(A-E)** Conditions known to bias SSRT estimates, including high RT skewness, RT
2059 slowdown, stop success rates, go omission rates, and context independence violations. **(F-I)**
2060 Additional conditions revealed by PRAD, such as high RT variability and kurtosis, high SSRT
2061 variability, and low SSD-SFR correlations. Higher PRAD SSRT estimates in these conditions
2062 demonstrate the model's ability to compensate for known biases and reveal new insights into
2063 SSRT estimation.

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Figure 16. Effect sizes for differences in PRAD parameters between different subgroups.
Each row reports the effect size for difference in the PRAD parameters and derived factors
between two subgroups. For instance, the first row depicts the effects sizes for differences in
parameters between participants who were identified as demonstrating violations of context
independence, and those who were not. These subgroups reflect the groups depicted in Figure 2.

Figure 17. Percentage reduction in typicality bias based on PRAD vs RVM control models.
The plots show the percentage reduction in typicality bias, measured as the reduction (from
RVM to PRAD) in residual errors in posterior model values of RT, SD(RT), SFR, and
correlation between SFR and SSD difference between atypical and typical populations. While
PRAD and RVM both demonstrate higher residual errors for atypical populations, PRAD
significantly reduces the gap in residual errors between atypical and typical populations, thus
debiasing inferences for atypical populations. Atypical populations tested here are based on
income (children from poorer families), age (younger children), CBCL externalizing (children
with CBCL externalizing t-scores > 64), cognitive abilities (children with lower cognitive scores
on the NIH cognitive toolbox), Brief Problem Monitoring survey (children with non-zero
scores), BISBAS scale (children with higher inhibition subscale scores), and ALE (children with
high bad event scores for adverse life events).

Figure 18. Predictive power of PRAD for NIH Toolbox cognitive tasks. Comparison of model fit and cross-validated performance using traditional SSRT (iSSRT) versus PRAD model parameters. Results show superior predictive power of PRAD for task-distal cognitive measures, with higher adjusted R² and correlations between predicted and actual values in both model fit and cross-validated analyses. Error bars show the 2.5th to 97.5th percentiles across 10-fold cross-validation.

Figure 19. Clinical relevance of PRAD model. (A) The bar charts show effects sizes for the traditional SSRT measure (iSSRT), and key PRAD measures related to proactivity and drift rates, for the effect between specific clinical groups and all other individuals. The clinical groups include attention disorders, rule-breaking, aggression, depression, ADHD, oppositional disorders, and conduct disorders, based on CBCL. In each case other than ADHD, iSSRT effect sizes are less than 0.2 (small). PRAD measures show small to medium (0.2 to 0.5) effect sizes for each of these clinical groups. **(B) Pairwise distance between clinical subgroups based on PRAD parameters**

Figure 20. Neural relevance of the PRAD model: Within-subjects analysis with PRAD
dynamic parameters reveals distinct neural correlates for reactive and proactive
mechanisms. (a-c) Whole-brain Cohen's d maps showing associations between trial-by-trial
brain activity and cognitive model parameters (SSRT, probability of proactivity, and proactive
delaying). Thresholded at Cohen's d ≥ 0.1. SSRT and probability of proactivity N = 4469;
proactive delaying N = 4176. **(d)** Network-level comparison of effect sizes based on the Shirer
parcellation(Shirer, Ryali, Rykhlevskaia, Menon, & Greicius, 2012). Error bars show 99%
confidence intervals computed using bootstrap resampling.

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2123 **Figure 21. Exposomic relevance of the PRAD model.**
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