The neuropeptide alpha calcitonin gene-related peptide impairs load-stimulated proteoglycan production of human chondrocytes via WNT activity

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Grant support: R1707/12-2 and GR1301/19-2 as part of ExCarBon (FOR2407) by the German Research Foundation

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Running title: aCGRP impairs load-stimulated proteoglycan production

ABSTRACT

Objective: Novel targets for osteoarthritis therapy are urgently needed, and

sensory nerve fibres and their neuropeptides are increasingly recognised for

their contribution to structural aspects of joint pathology. The nociceptive

sensory neuropeptide alpha calcitonin gene-related peptide (αCGRP) was

previously detected in synovial fluid and serum of osteoarthritis patients and

was also described as trophic factor for chondrocytes, affecting ECM

organisation and biomechanical properties. Here, we investigated the

potential of αCGRP to alter the chondrocyte mechanoresponse, and thus to

affect the resilience of cartilage towards mechanical loading.

Methods: Tissue-engineered neocartilage based on human articular

chondrocytes was treated with 1μM αCGRP for 24 hours and subjected to an

anabolic loading protocol (intermittent dynamic compression, 1Hz, 25%) for

the last 3 hours before analysing its molecular mechano-response.

Results: Mechanotransduction was largely unaltered by αCGRP as

demonstrated by ERK activation and stimulation of mechano-regulated gene

expression, yet load-stimulated glycosaminoglycan synthesis was disturbed

by αCGRP. Presence of αCGRP did not affect stimulation of *WNT5A*

expression by loading, but decreased *DKK3* expression under loading.

Importantly, WNT inhibition prevented the negative effect of αCGRP on load-

stimulated glycosaminoglycan synthesis.

Conclusion: Identifying *WNT5A* as a novel mechano-response gene, we

reveal that αCGRP can block the load-stimulated proteoglycan production of

human chondrocytes in the presence of WNT pathway activity. Thus, our data

propose a novel, negative role for the pain-mediator αCGRP in the cartilage

loading response, compromising its resilience to loading. Overall, our study

implicates αCGRP as a potential target for osteoarthritis treatment, but also in

patient stratification.

Keywords: cartilage, aCGRP, osteoarthritis, mechanical loading, WNT

signalling.

INTRODUCTION

Osteoarthritis (OA) is a leading cause of disability, with 7.6 % of the global

population (nearly 600 million people) living with some form of OA in 2020[1].

During OA, the structural and functional properties of joint tissues, including

articular cartilage, are progressively compromised, resulting in symptoms

such as joint stiffness, immobility and pain. Whilst the burden of disease is

predicted to rise further by 2050, there is no effective cure for OA and despite

intense efforts, no disease-modifying osteoarthritis drugs (DMOADs) have

been approved by regulatory agencies to date[2]. Thus, there is an urgent need

to identify novel potential targets for OA prevention and therapy. Importantly,

physiological mechanical stimulation contributes to cartilage homeostasis and

maintenance[3-5]; however, cartilage degeneration during OA impairs this

functional capacity to withstand and adequately transmit mechanical forces

during joint movement, affecting its resilience towards mechanical loading[2].

An improved understanding of the molecular chondrocyte loading response

and how it is affected by degenerative changes within the joint could therefore

reveal novel approaches to enhance the resilience of (OA) cartilage towards

mechanical loading and thereby slow or prevent disease progression.

Sensory nociceptive nerve fibres are increasingly recognised for their

contribution to joint pathology, but whether they compromise the

mechanoresponse of cartilage in an aching joint currently remains unknown.

Atypical innervation of joint tissues including the typically aneural cartilage has

been reported in OA[6, 7], and some studies suggested a correlation between

sensory nerve fibre innervation, OA severity and OA-related pain[7-9]. These

nerve fibres secrete sensory neuropeptides, such as *α calcitonin gene related*

peptide (αCGRP), a 37 amino acid peptide best known as pain-mediator[10]. Of

note, previous studies have reported elevated levels of αCGRP in serum,

plasma and synovial fluid from patients with painful knee OA[11-14], indicating

that there are several potential cellular sources of αCGRP within the (OA)

joint. Whilst αCGRP levels were suggested to correlate with OA pain and

severity, sensory neuropeptides including αCGRP have also been described

to act as trophic factors for several cell types of the joint, including osteoblasts

and chondrocytes[15-17], lending support to a potential active role of αCGRP as

a driver of OA pathology, and a decrease in load resilience.

Some insights into potential functions of αCGRP in joint homeostasis and

pathology come from recent animal and in vitro studies. Mice deficient for

αCGRP were protected from age-related knee OA[18], whereas cartilage

degeneration was accelerated following surgical induction of OA in the

absence of αCGRP[17]. Nevertheless, pharmacological inhibition of αCGRP via

receptor antagonists attenuated OA progression following surgical OA

induction[19, 20], suggesting a context-dependent function of αCGRP in

cartilage. When surgical OA-induction was followed by intense exercise,

extracellular matrix (ECM) stiffening was prevented in αCGRP-deficient

mice[21], revealing effects of αCGRP on ECM organisation and biomechanical

properties in vivo. Previous work reported a link between the mechano-

response of cartilage and the sensory neuropeptide Substance P[22], and so

we asked whether the molecular response to mechanical loading may be

altered by the presence of αCGRP.

Studies on the chondrocyte loading response typically employ cartilage

explants or tissue-engineered 3D cartilage subjected to a strictly defined

loading protocol in vitro. We have previously established a loading regimen

which elicits an anabolic response in tissue-engineered cartilage, as

demonstrated by increased proteoglycan synthesis rates on the metabolic

level and by whole-transcriptome analysis[23]. In addition to increased

extracellular signal-regulated kinase (ERK) phosphorylation and elevated

expression of *FOS* and *PTGS2*, which are mechano-regulated in various

tissues[24-28], we also demonstrated enhanced *BMP2* and *BMP6* expression,

and increased SRY-box transcription factor 9 (SOX9) protein levels, in line

with the observed anabolic response of chondrocytes to the chosen loading

regimen[23]. In agreement with studies employing different models and loading

protocols[29], we also reported that the cartilage ECM is a crucial parameter of

the chondrocyte loading response[30]. Importantly, tissue-engineered cartilage

allows the use of human cells and the accumulation of cartilage-like ECM,

whilst also permitting defined culture and mechanical loading conditions,

therefore filling an important gap between highly complex animal models and

classical 2D cell culture experiments.

Here, we used this established model system to address whether αCGRP

alters the molecular loading response of chondrocytes, and whether this can

contribute to a decreased resilience of cartilage towards mechanical loading

by investigating mechano-regulated signalling and the metabolic response of

human chondrocytes in the presence of αCGRP. Tissue engineered

neocartilage generated from human articular chondrocytes was exposed to

αCGRP and subjected to a physiologically relevant anabolic loading regimen

known to stimulate glycosaminoglycan (GAG) synthesis[23, 30]. The molecular

response of untreated or αCGRP-treated neocartilage was then examined by

qRT-PCR, western blotting and radiolabelling. A direct functional effect of

αCGRP on the chondrocyte response to physiologically relevant mechanical

stimulation has the potential to lead to novel approaches for OA treatment.

METHODS

Isolation and expansion of articular chondrocytes

Articular cartilage samples were obtained from 14 donors (3 males, 11

females, 52 – 87 years of age, mean age 66.9 years) undergoing total knee

replacement surgery with informed written consent of the patients. The study

was approved by the local ethics committee on human experimentation of the

Medical Faculty of Heidelberg and in agreement with the Helsinki Declaration

from 1975 (latest version). Articular chondrocytes (ACs) were isolated from

macroscopically intact cartilage as described previously[23, 30]. Cells were

expanded in DMEM containing 1 g/L glucose, 10 % FBS, 1 %

penicillin/streptomycin and 2 mM L-glutamine (all Gibco^{TM}, ThermoFisher

Scientific, Germany) for two passages.

Generation of tissue-engineered neocartilage

In order to generate neocartilage, ACs were seeded onto type I/III collagen

carriers (4 mm diameter, 1.5 mm height, Optimaix, Matricel, Germany) at

5×10^5 cells/construct, attached to a glass carrier (ROBU, Germany) to mimic

the subchondral bone (bone replacement phase) and cultured for 35 days as

described previously[23, 30] using chondrogenic medium: DMEM (4.5 g/L

glucose, 2 mM L-glutamine, Gibco[TM], ThermoFisher Scientific), 1 %

penicillin/streptomycin (Gibco[TM], ThermoFisher Scientific), 0.1 mM

dexamethasone, 0.17 mM ascorbic acid-2-phosphate, 2 mM sodium pyruvate,

0.35 mM proline, 5 µg/mL transferrin, 5 ng/mL sodium selenite, 1.25 mg/mL

bovine serum albumin (all Sigma-Aldrich, Germany), 5 µg/mL insulin (Lantus,

Sanofi-Aventis, Germany) and 10 ng/mL TGF-β1 (#100-21-100UG,

Peprotech, Germany). 1 µM αCGRP (#4013281, Bachem, Germany) was

added for the last 24 h of culture where indicated.

Cyclic unconfined dynamic compression of neocartilage

Neocartilage was exposed to a single 3 h episode of mechanical loading in a

custom-designed bioreactor with the dynamic compression protocol carried

out using the software Galil Tools as described previously[23, 30]. In brief,

neocartilage was initially compressed by 10 % of its thickness to ensure the

constant contact with the piston during compression. Starting from this 10 %

static offset, neocartilage was compressed by 25 % at 1 Hz during the loading

intervals (10 min) whilst maintaining the offset of 10 % during break intervals

(10 min). After loading, samples were washed in PBS and snap frozen, or

used for metabolic labelling analysis. 1 µM αCGRP and where indicated 2 µM

IWP-2 (Tocris, Germany) were added 21 h before start of compression and

treatment was continued during loading and subsequent metabolic labelling.

Radiolabel incorporation, glycosaminoglycan and DNA quantification

GAG synthesis was analysed after the end of loading as described

previously[30]. Engineered tissue was labelled with 4 µCi ^{35}S as Na_2SO_4

(Hartmann Analytic, Germany) for 24 h in 500 µL chondrogenic medium with

or without treatments. Labelled neocartilage was then washed and digested

with proteinase K (ThermoFisher Scientific) overnight. Incorporated radiolabel

was measured in tissue lysates by β-scintillation counting (1414 WinSpectral,

PerkinElmer, Germany) and normalised to the DNA content of the same

lysates. DNA content was determined using Quant iT Pico Green Kit

(Invitrogen, Germany). Total GAG content of each sample was determined by

1,9-dimethylmethylene blue (DMMB) assay using a chondroitin-6-sulfate

standard (Sigma-Aldrich).

RNA isolation and mRNA expression analysis

Total RNA was isolated from neocartilage using Trizol (Life Technologies,

Germany). 500 ng of total RNA was reverse transcribed using Omniscript RT

Kit (Qiagen, Germany) and oligo(dT) primers. Gene expression was analysed

by qRT-PCR (Roche Diagnostics, Germany) using SYBR green

(ThermoFisher Scientific). *CPSF6* and *HNRPH1* were used as housekeeping

genes. Primer sequences are listed in table S1.

Western blotting

Neocartilage was cut in half and ground in PhosphoSafe Extraction Reagent

(Merck Millipore, Germany) containing 1 mM Pefabloc SC (Sigma-Aldrich,

Germany) in a mixer mill (Retsch, Germany) at 30 Hz for 2 x 2 min, with

cooling on ice in between cycles. Samples were centrifuged at 13000 x g for

20 min at 4°C before cell lysates were mixed with 4 x Laemmli buffer and

boiled for 5 min at 95°C. Proteins were separated according to size using

standard SDS-PAGE and transferred onto a nitrocellulose membrane (GE

Healthcare, Amersham, Germany). Membranes were blocked in 5 % skimmed

milk/TBS-T and probed with primary antibodies (see table S2) at 4°C

overnight. Detection was carried out using horseradish peroxidase-conjugated

secondary antibodies (see table S2) and enhanced chemiluminescence

(Roche Diagnostics, Germany/Advansta, USA). Densitometric analysis was

performed using ImageJ.

Histology

Neocartilage was separated from the bone replacement phase and fixed in 4

% PFA for 4 h at room temperature. After dehydration in an ascending

isopropanol series, samples were embedded in paraffin wax for slide

preparation. After rehydration, proteoglycan deposition was analysed by

staining 5 µm sections with 0.2 % safranin-O (Fluka, Sigma-Aldrich,

Germany) in 1 % acetic acid and counterstaining with 0.04 % Certistain fast

green (Merck, Germany) in 0.2 % acetic acid. Type II collagen

immunostaining was performed as follows: Sections were rehydrated and

digested with hyaluronidase (Roche Diagnostics, Mannheim, Germany, 4

mg/mL in PBS, pH 5.5) followed by pronase (Roche Diagnostics, 1 mg/mL in

PBS, pH 7.4), before unspecific binding sites were blocked using 5 % BSA.

After incubation with mouse anti-human type II collagen antibody (see table

S2), sections were incubated with ALP-coupled anti-mouse secondary

antibody (see table S2), and ImmPACT® Vector® Red Substrate (Vector

Laboratories, Newark, CA, USA). As negative controls, undifferentiated stem

cells cultured in a collagen carrier were used, in addition to a type II collagen-

positive neocartilage sample stained without primary antibody (see Fig. S1B).

Statistical analysis

Statistical analysis was performed using IBM SPSS Statistics (29.0.0.0). Fold

changes were calculated relative to the respective free-swelling samples and

P-values calculated using appropriate statistical testing as noted in the figure

legends, with *P* < 0.05 considered statistically significant.

RESULTS

Neocartilage quality is sustained in the presence of αCGRP

In order to investigate the effect of αCGRP on the immediate molecular

response of chondrocytes to mechanical loading, we chose to limit the

αCGRP treatment to the last 24 h of culture, including the dynamic unconfined

compression on day 35, thus avoiding previously reported reductions in GAG

deposition following αCGRP treatment for 7 days[31]. At the end of culture,

untreated   and   αCGRP-treated   neocartilage   was   histologically

indistinguishable (Fig. 1A), with both groups exhibiting comparable, strong

GAG and type II collagen staining. Accordingly, the GAG synthesis rate as

well as total GAG content was generally maintained in the presence of

αCGRP (Fig. 1B). No significant changes were observed in the DNA content

of control or αCGRP-treated neocartilage (Fig. S1A). Similar expression levels

of the chondrocyte marker genes *COL2A1*, *ACAN* and *SOX9* between control

and αCGRP-treated samples (Fig. 1C) also indicated that short-term αCGRP

treatment did not exert significant negative effects on neocartilage.

Figure 1 – Neocartilage ECM structure and quality is sustained in the presence of αCGRP. Articular chondrocytes were cultured in collagen carriers for 35 days and treated with 1 µM αCGRP for the last 24 h of culture. (A) Histological staining of glycosaminoglycans (GAG) by safranin-O/fast green staining and of type II collagen by immunohistochemistry (IHC). Positive and negative controls for IHC are provided in the supplements (Fig. S1B). N = 5 donors. Scale bar: 500 µM unless otherwise stated. (B) GAG synthesis over 24 h was assessed by radiolabelling using ^{35}S-sulfate ($Na_2{}^{35}SO_4$). Changes in ^{35}S-sulfate incorporation were normalised to DNA content (measured by PicoGreen assay). GAG content was determined using the DMMB method and normalised to the DNA content. N = 8 donors. (C) Expression of chondrocyte marker genes *COL2A1, ACAN,* and *SOX9* was quantified by

qRT-PCR using *CPSF6* and *HNRPH1* as reference genes. N = 7 donors.

Bars represent the median value.

αCGRP does not impair chondrocyte mechano-transduction

Next, day 35 neocartilage tissue constructs were subjected to a previously

established anabolic loading protocol consisting of 3 h of dynamic unconfined

compression in the presence or absence of αCGRP. In order to assess the

chondrocyte mechano-transduction response, phosphorylation of the MAP

kinase ERK1/2 was examined by western blotting (Fig. 2A). As expected,

mechanical loading significantly enhanced ERK1/2 phosphorylation in the

control group. ERK1/2 phosphorylation was also significantly stimulated in the

presence of αCGRP. We then examined expression levels of known

mechano-regulated genes, including *FOS* and *PTGS2* (Fig. 2B). Expression

of both genes was significantly enhanced following mechanical loading, in the

control group (median fold change 4.61 and 4.72, respectively) as well as in

the presence of αCGRP (median fold change 4.12 and 3.91, respectively).

Furthermore, SOX9 protein levels were significantly increased by mechanical

loading, both in the presence as well as absence of αCGRP (Fig. 2C). This

was also reflected in upregulated mRNA levels (Fig. S2), in line with our

previous reports[23]. Furthermore, *BMP2* and *BMP6* expression was stimulated

by mechanical loading in both groups (Fig. 2D). Since these known mechano-

regulated factors still responded to compression in the presence of αCGRP,

we concluded that chondrocyte mechano-transduction was generally not

affected by the presence of αCGRP.

Figure 2 – Chondrocyte mechano-transduction is not altered by αCGRP. Neocartilage was subjected to 3 h of mechanical loading in the presence or absence of 1 µM αCGRP, added for the last 24 h of culture (including the loading period). (A) Visualisation and quantification of ERK phosphorylation by western blotting. Densitometric analysis was performed in ImageJ using β-actin as loading control and the fold change calculated relative to the non-loaded control set to 1. (B) Gene expression analysis of *FOS* and *PTGS2* by qRT-PCR, using *CPSF6* and *HNRPH1* as reference genes, and fold changes calculated relative to the non-loaded control set to 1. (C) Visualisation and quantification of SOX9 protein levels by western blotting. Densitometric analysis was performed as above. (D) Gene expression analysis of *BMP2* and *BMP6* by qRT-PCR, using *CPSF6* and *HNRPH1* as reference genes, and fold changes calculated relative to the non-loaded control set to 1. N = 6-7 donors. Bars represent the median value. P-values were calculated using Mann-Whitney-U testing with the non-loaded control set to 1, * indicate p < 0.05, **

indicate p < 0.01, *** indicate p < 0.001. Uncropped images of western blot

membranes are provided in the supplemental information (Fig. S5).

Load-stimulated proteoglycan production is disturbed by αCGRP

The impact of αCGRP treatment on the functional response of chondrocytes

was assessed by performing ^{35}S-sulfate isotope labelling of newly

synthesised GAGs over 24 h after the end of loading (Fig. 3A). In the control

group, dynamic compression resulted in significantly enhanced GAG

synthesis by an average of 24.7 %, a value in agreement with our previous

studies[30]. Although no major alterations in mechano-transduction or

mechano-regulated gene expression were observed after αCGRP treatment,

the stimulation of GAG synthesis following loading was clearly disrupted (Fig.

3A). DNA content per sample and total GAG content were maintained in both

control and αCGRP-treated neocartilage following loading, indicating that the

αCGRP effect was not due to tissue disruption (Fig. 3B, C). Furthermore, the

effect of αCGRP on load-mediated GAG synthesis stimulation appeared

dose-dependent in a smaller set of experiments (Fig. S3).

Figure 3 – Load-stimulated GAG synthesis is disturbed by the presence of αCGRP. Neocartilage was subjected to 3 h of mechanical loading in the presence or absence of 1 μM αCGRP, added for the last 24 h of culture. (A) GAG synthesis was assessed by radiolabelling for 24 h after loading using ^{35}S-sulfate (Na$_2$^{35}SO$_4$). ^{35}S-sulfate incorporation was normalised to DNA content and referred to the non-loaded control set to 1. (B) DNA content, measured by PicoGreen assay was assessed following radiolabelling and normalised to the non-loaded control set to 1. (C). Total GAG content was quantified by the DMMB method, normalised to the DNA content per sample, and referred to the non-loaded control set to 1. N = 8 donors. Bars represent the median value, p-values were calculated using Mann-Whitney-U testing with the control set to 1, *** indicate p < 0.001.

αCGRP-induced disruption of proteoglycan production after mechanical

loading is alleviated by WNT inhibition

We then explored the mechanism by which αCGRP interferes with load-

induced GAG synthesis. Our previous studies identified a precise regulation of

WNT activity as crucial factor for the chondrocyte loading response[30] and in

human osteoblasts, treatment with αCGRP was previously described to result

in the stabilisation of the central WNT mediator β-catenin[16]. Therefore, we

next examined whether the presence of αCGRP during mechanical loading

affects the WNT signalling network of human neocartilage. Amongst WNT

ligands expressed in human chondrocytes according to our previously

published data[32], WNT5A inhibited anabolic gene expression in human

chondrocytes[33]. Interestingly, several studies on human tenocytes revealed

an upregulation of *WNT5A* in response to mechanical stimulation[34, 35]. Thus,

we examined whether gene expression of *WNT5A* was regulated following

mechanical loading in control and αCGRP-treated neocartilage (Fig. 4A).

Indeed, *WNT5A* mRNA levels were significantly elevated following

mechanical loading in both groups (median fold change 1.38 and 1.42,

respectively). Of note, the amount of another chondrocyte-expressed WNT

ligand (*WNT11*)[32] remained unchanged by mechanical loading in the

presence or absence of αCGRP. We also examined the expression of the

WNT antagonist *DKK3,* the only expressed form of dickkopf under the chosen

conditions according to our previous array data[32]. DKK3 has previously been

described to prevent cytokine-induced proteoglycan loss and WNT-induced

proteoglycan reduction[36]. Whilst mechanical loading had no significant effect

on *DKK3* expression in the non-treated control group (median fold change

0.86), *DKK3* transcript levels were significantly reduced by nearly 40 % when

mechanical loading was performed in the presence of αCGRP (median fold

change 0.61, $p < 0.001$). Treatment with αCGRP alone did not significantly

alter expression of *WNT5A, WNT11* or *DKK3* compared to non-loaded control

neocartilage (Fig. S4A).

In order to investigate whether αCGRP exerts its effect on proteoglycan

production via modulation of WNT signalling, neocartilage was subjected to

dynamic compression in the presence of αCGRP, and additionally treated

with the pan-WNT inhibitor IWP-2 (2 µM) or DMSO as solvent control. Neither

DNA content nor GAG/DNA ratio were significantly altered following IWP-2

treatment, αCGRP treatment, or co-treatment (Fig. S4B, C). As expected,

GAG synthesis was stimulated by mechanical loading in the control group (on

average by 38%), as well as in the presence of IWP-2, whereas αCGRP

prevented this response (Fig. 4B). Strikingly, the inhibitory effect of αCGRP

on the stimulation of GAG synthesis following compression was alleviated in

the presence of IWP-2 (average stimulation of 36 %). Together, these data

reveal that αCGRP can disturb chondrocyte proteoglycan production in

response to anabolic loading by interfering with the delicate balance of WNT

signalling activity in cartilage. Thus αCGRP at least partly impairs the

mechano-adaptive response of chondrocytes to mechanical stimulation.

Figure 4 – WNT inhibition alleviates αCGRP-mediated restriction of

proteoglycan production. Neocartilage was subjected to 3 h of mechanical

loading with 1 µM αCGRP and 2 µM IWP-2 added for the last 24 h of culture

where indicated. (A) Gene expression analysis by qRT-PCR, using *CPSF6*

and *HNRPH1* as reference genes and fold changes calculated relative to the

non-loaded control set to 1. N = 7 donors. (B) GAG synthesis was assessed

by radiolabelling using ^{35}S-sulfate ($Na_2{}^{35}SO_4$). Changes in ^{35}S-sulfate

incorporation were normalised to DNA content and referred to the non-loaded

control set to 1. Bars represent the median value. N = 5-6 from 4-5 donors. P-

values were calculated using Mann-Whitney-U testing with the control set to

1, * indicate p < 0.05, ** indicate p < 0.01, *** indicate p < 0.001.

DISCUSSION

DISCUSSION

Responding adequately to mechanical loading is an important function of

articular cartilage, which is impaired by degenerative processes during OA

and thus renders cartilage less resilient towards mechanical challenge.

Illuminating the effects of OA-relevant changes on the response of

chondrocytes to mechanical stimulation has the potential to identify novel

causative therapeutic targets and may suggest new strategies of stratifying

patients who can especially benefit from a specific therapy. Previous reports

suggested a correlation between αCGRP levels and OA pain[11, 13, 14], and in

vivo studies employing mouse models revealed roles for αCGRP also in

structural aspects of joint pathology[15, 17, 18, 21]. Yet, the effects of αCGRP on

functional aspects of cartilage, such as the chondrocyte loading response,

have remained so far unaddressed. In our present study, we reveal that

αCGRP can compromise the anabolic response of chondrocytes to a

physiological loading regimen, and thus the resilience of cartilage towards

mechanical loading. We further show that WNT inhibition alleviates this effect

of αCGRP, altogether suggesting αCGRP as a potential target for OA

treatment.

Our study employed a previously established and well characterised tissue-

engineering model based on human chondrocytes[23, 30], which allows their

mechanical stimulation under defined experimental conditions. Thus, we were

able to investigate important functional aspects of human cartilage biology,

thereby filling the large gap between the complex in vivo environment and

oversimplified (2D) cell culture models. By limiting the duration of αCGRP

exposure, we prevented significant effects on proteoglycan accumulation by

αCGRP treatment alone as described by an earlier study[31], allowing us to

identify how αCGRP influences the chondrocyte loading response.

Importantly, the selected loading regimen reflects physiological loading

conditions by employing an intermittent compression protocol, and presents

an anabolic stimulus[23]. This model therefore provided the exciting opportunity

to assess whether αCGRP can alter the metabolic response of chondrocytes

to physiological mechanical loading under defined and strictly-controlled

conditions.

Using this model, we demonstrated for the first time that αCGRP disrupted the

stimulation of GAG synthesis by mechanical loading, suppressing the

anabolic effect of this physiological loading regimen. Our current data provide

novel and compelling evidence to implicate αCGRP in a reduced load

resilience of cartilage, further supporting functional contributions of sensory

neuropeptides to cartilage homeostasis, but also to cartilage degeneration

during OA and suggesting αCGRP as a potential therapeutic target. Specific

αCGRP-targeted therapeutics are already approved for unrelated conditions

including migraines (as reviewed in[37]). Our findings are in line with previous

studies using human chondrocytes under static conditions, which revealed

reduced GAG deposition in the presence of αCGRP[31] as well as studies

employing animal models, which linked αCGRP to changes in ECM

organisation and biomechanical properties[17, 21]. In vivo studies also revealed

that αCGRP-deficiency protected knee cartilage from degradation in a mouse

model of age-related OA[18], and pharmacological inhibition of αCGRP also

attenuated cartilage degeneration following surgical induction of OA[19, 20]. Yet,

life-long αCGRP-deficiency enhanced cartilage degeneration following

induction of post-traumatic OA[17], and intra-articular injection of αCGRP-

overexpressing bone marrow stromal cells following surgical OA induction

appeared to have beneficial effects on general mobility and activity in a

mouse model[38]. Genetic ablation of αCGRP is known to result in

osteopenia[15], and altered homeostatic conditions within the joint may explain

these discrepancies. Still, further studies into the context-dependent

regulation of αCGRP as an active driver of OA pathology are required to

resolve these apparent contradictions.

Importantly, our study linked the effect of αCGRP in the context of mechanical

loading to WNT activity. The WNT signalling pathway is well-known for its

contribution to cartilage degeneration and OA pathology[39] and during our

previous study, stabilisation of the WNT-mediator β-catenin prevented the

anabolic response of chondrocytes to the chosen loading episode[30].

Conversely, a pan-WNT inhibitor rescued the load-induced reduction of GAG

synthesis in presence of high WNT/β-catenin levels as a potent negative

regulator of load-induced chondrocyte anabolism. Additionally, αCGRP was

previously reported to contribute to a stabilisation of β-catenin in

osteoblasts[16], in line with pro-anabolic effects of αCGRP in bone in vivo[15].

Here, we applied this knowledge to mitigate the effect of αCGRP on GAG

synthesis stimulation following mechanical loading, using the WNT inhibitor

IWP-2. Since IWP-2 acts via blocking the secretion of endogenously produced

WNT ligands, our data implicate a WNT ligand-mediated pathway in the

action of αCGRP.

Which WNT ligands are involved in chondrocyte mechano-transduction and in

mediating the effect of αCGRP remains to be elucidated in future studies.

Here, we report for the first time elevated expression of the non-canonical

WNT ligand *WNT5A* as a novel mechano-response gene of human

chondrocytes. *WNT5A* was recently identified as an effector gene in

osteoarthritis[40]. Increased expression of *WNT5A* has also been described in

response to cyclic stretch and tensile strain in human tenocytes as well as

human mesenchymal stromal cell-derived tenocytes and murine superficial

zone chondrocytes[34, 41]. Importantly, our previous transcriptome-wide study[23]

revealed the mechano-regulation of known WNT target genes, but the

responsible ligand remains unknown. Other studies have also described

WNT/β-catenin activity following mechanical loading of chondrocytes[42];

however, the mediating ligand was also not identified. It remains to be

addressed by future studies whether the mechano-regulation of *WNT5A*

contributes to WNT activity in chondrocytes, and whether this involves β-

catenin-dependent or -independent mechanisms. Importantly, in αCGRP-

treated neocartilage, mechanical loading resulted in a concurrent decrease in

DKK3 expression. Depending on the biological context, DKK3 has been

described as non-canonical or canonical WNT inhibitor; however, at least one

previous study has shown that DKK3 can antagonise the archetypal canonical

WNT ligand WNT3A in human chondrocytes[36]. It is tempting to speculate that

a reduction in *DKK3* expression, but sustained upregulation of *WNT5A* in the

presence of αCGRP could result in an altered balance of non-canonical vs

canonical WNT activity following mechanical loading, and that this could

contribute to a decreased resilience of cartilage towards mechanical loading.

Our findings implicating WNT activity as a mediator of αCGRP could also be

relevant for patient stratification. Whilst patient heterogeneity as well as

insufficient stratification of patient subgroups and phenotypes remain a major

problem in the development and clinical testing of DMOADs, one of the very

few substances that have progressed into advanced clinical trials (reviewed

in[43]), lorecivivint, was described to modulate WNT activity[44, 45]. Thus, it would

be interesting to investigate whether lorecivivint is able to mitigate the effect of

αCGRP on proteoglycan production following mechanical loading. This

knowledge could link the potential DMOAD to an improved resilience of

cartilage towards mechanical loading. Since αCGRP has already successfully

been detected in synovial fluid and serum samples from OA patients,

increased αCGRP levels could possibly identify patients that would benefit

particularly from WNT activity modulation.

Our study has several limitations. Since we performed the αCGRP treatment

after formation of a cartilage ECM, we used a supra-physiological

concentration of αCGRP, which is higher than concentrations used in other

studies using human chondrocytes[31]. However, in contrast to other studies,

which have applied αCGRP during the entire culture period, we added

αCGRP to already matured neocartilage and therefore raised the

concentration in order to ensure penetration of the dense, collagen- and

proteoglycan-rich extracellular matrix. Another limitation is that we tested the

effect of αCGRP treatment only in combination with one physiological loading

regime. Future studies are required to assess the effects of other types of

loading protocols (such as mechanical overloading), and multi-axial loading

conditions in the presence of αCGRP. It is also important to note that WNT

activity-related β-catenin is typically analysed following the saponin extraction

method[46] to eliminate membrane-bound β-catenin involved in cell adhesion;

however, the dense structure of (tissue-engineered) cartilage is incompatible with this extraction method, which precluded the analysis of β-catenin levels. Lastly, we relied on the generous tissue donations from OA patients undergoing total knee replacement surgery, so chondrocytes were derived from OA patients; however, we took this into account during experimental design and strictly limited exposure to αCGRP in order to prevent the effects on proteoglycan accumulation described for OA but not non-OA chondrocytes[31].

In conclusion, we showed here for the first time that the sensory neuropeptide αCGRP, which was previously implicated in OA progression, can impair load-stimulated proteoglycan production by human chondrocytes, and thus interferes with their anabolic response to physiological mechanical loading. Our findings indicated that αCGRP can compromise the resilience of cartilage towards mechanical loading, and linked this effect of αCGRP to WNT activity. We also report *WNT5A* as a novel mechano-response gene in human chondrocytes. Overall, our data support a role for αCGRP in cartilage degeneration and OA progression and as a potential new therapeutic target. Elevated αCGRP levels may also help stratifying patients that can benefit from a WNT antagonistic treatment.

Acknowledgements

We thank Dr. Christian Kleist and Nadine Weissheimer for their generous assistance with liquid scintillation counting, Barbara König, Elena Tripel and Sarina Losch for excellent technical assistance, the surgical staff for support with sample collection, and I. Heschel from Matricel for providing the Optimaix scaffolds. We would also like to thank Dr. Sabine Stöckl for helpful advice.

This study was supported by the German Research Foundation DFG-grant

R1707/12-2 and GR1301/19-2 as part of the Excarbon Research Group

FOR2407, the University of Regensburg and the Orthopaedic University

Hospital Heidelberg.

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Nicole Hecht: Investigation, Conceptualisation, Methodology, Formal

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Role of the funding source

This study was supported by the German Research Foundation DFG-grant

R1707/12-2 as part of the ExCarBon Research Group FOR2407 and the

Orthopaedic University Hospital Heidelberg.

Competing interest statement

The authors declare no conflicts of interest.

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