Region-specific spreading depolarization drives aberrant post-ictal behavior

Bence Mitlasoćzki[1,2], Adrián Gutiérrez Gómez[1], Midia Kamali[1,2], Natalia Babushkina[3,4], Mayan Baues[1,2], Laura Kück[1,2], André Nathan Haubrich[2], Theodoros Tamiolakis[1,2], Annika Breuer[1], Šimon Granak[1], Merlin Schwering-Sohnrey[1,2], Ingo Gerhauser[5], Wolfgang Baumgärtner[5], Laura Ewell[6], Thoralf Opitz[2], Julika Pitsch[1], Simon Musall[2,3,4], Rainer Surges[1], Florian Mormann[1], Heinz Beck[2,7], Michael Wenzel[1,2*]

University Hospital Bonn, Dept. of Epileptology, Bonn, Germany
University of Bonn, Medical Faculty, Institute of Experimental Epileptology and Cognition Research, Bonn, Germany
Institute of Biological Information Processing (IBI-3) – Bioelectronics Forschungszentrum, Jülich, Germany
Institute of Biology II, RWTH Aachen University, Aachen, Germany
Department of Pathology, University of Veterinary Medicine Hannover, Hannover, Germany
Department of Anatomy and Neurobiology, University of California, Irvine, USA
Deutsches Zentrum für Neurodegenerative Erkrankungen e.V., Bonn, Germany

*Correspondence to:
Michael Wenzel
University Hospital Bonn, Dept. of Epileptology, Venusberg-Campus 1, 53127 Bonn, Germany
Email: michael.wenzel@ukbonn.de
Phone: +49 228 287 16954

Number of main figures: 4
Number of suppl. figures/tables: 9/2

Author approvals: All authors have seen and approved the manuscript, and the manuscript has not been accepted or published elsewhere.

Conflict of Interest: The authors declare no competing interests.

Summary

Confusion, aphasia, and unaware wandering are prominent post-ictal symptoms regularly observed in temporal lobe epilepsy (TLE)[1]. Despite the potentially life-threatening nature of the immediate post-ictal state[2], its neurobiological underpinnings remain understudied[3]. We provide evidence in mice and humans that seizure-associated focal spreading depolarization (sSD) is a pathoclinical key factor in epilepsy. Using two-photon or widefield imaging (hippocampus, neocortex), field potential and single unit recordings, and behavioral assessment in mice, we first studied seizures during viral encephalitis, and subsequently established an optogenetic approach to dissociate hippocampal seizures and SD. We find region-specific occurrence of sSD that displays distinct spatial trajectories to preceding seizures, and show that seizure-related and isolated hippocampal SD prompt *post-ictal wandering*. This clinically relevant locomotor phenotype occurred in the absence of hippocampal SD progression to the neocortex. Finally, we confirm sSD existence in human epilepsy, in a patient cohort with refractory focal epilepsy, via Behnke-Fried electrode recordings. In this cohort, sSD displayed a similar temporomesial propensity as in mice. This work uncovers sSD as a previously underrecognized pathoclinical entity underlying postictal behavioral abnormalities in epilepsy. Our results carry wide-reaching ramifications for epilepsy research and neurology, and challenge current EEG-standards.

Introduction

The immediate post-ictal period often manifests with confusion, aphasia, amnesia, or unaware ambulation (*post-ictal wandering*), which is most commonly observed in temporal lobe epilepsy (TLE)[1,3]. It is associated with a risk for severe, potentially life-threatening injuries[2]. Despite its clinical impact, except for particular entities such as sudden unexpected death in epilepsy (SUDEP)[4,5], the neurobiological underpinnings of the immediate post-ictal state remain unclear, and most related research on this topic has focused on consequence rather than initial cause[6,7]. One reason for the continued scarcity of neurobiological insight may be that the *ictus* itself has continually formed the center of interest in epilepsy research and clinical care, which is also reflected in clinical terminology (ictus, ictal, pre-/post-/peri-ictal).

Previous work has suggested that network dynamics other than seizures (Sz), e.g. spreading depolarization/depression (SD)[8], could in principle account for a number of post-ictal symptoms[3,4,9]. Most of what is known about SD stems from research on migraine, stroke and traumatic brain injury[10–12]. In the latter context, Sz and neocortical SD have been investigated also in clinical electrical recordings[13–22]. While generally, SD has been recorded in hippocampus[23–29], thalamus[30,31], basal ganglia[23], or brainstem[4,5], the vast majority of SD research has focused on neocortex, which brought about the common term cortical spreading depression (CSD)[32]. Put simply, SD constitutes a massive ion translocation across the neuronal cell membrane resulting in a profound depolarization above the inactivation threshold, a break-down of the membrane potential and consecutive neuronal depression[8,32,33]. SD can be elicited in various ways, e.g. by

energy depletion[34–36], hypoxia[37], high extracellular K^{+}[36,38–40], repetitive electrical or

mechanical stimulation[8], or optogenetic neuronal depolarization[41–46]. Depending on the

etiology, SD has profound effects on affected brain tissue such as transient edema and

vasoconstriction, danger molecule release in the extracellular space (i.e. ATP), or

immune activation[12,26,37,47]. Such effects may be transient and recovered from, but can

also lead to permanent tissue damage[21,48].

While some of the mentioned studies have documented an association of SD and Sz in

acute brain injury in neurointensive care[15,18], it is unknown whether Sz-related SD exists

in human epilepsy at the clinical level. In basic epilepsy research, the role of SD remains

debated. SD has both been suggested to increase neural excitability[29,49], and to disrupt

ictal oscillations[27,50,51]. Some have speculated about a protective role of SD in

epilepsy[50,52], while others have described Sz-related SD as a potential cause for SUDEP

via brain stem invasion[4,5]. Certainly, as most basic research on Sz-related SD has been

carried out in vitro, or under anesthesia[8,9,23,26,49,50], the general relationship between Sz-

related SD and potentially distinct clinical symptoms have remained understudied. In

current clinical epileptology, concepts revolving around Sz-related SD, aside from

SUDEP, play little to no role.

Here, we provide *in-vivo* evidence in mice and humans that Sz-associated focal spreading

depolarization (sSD) constitutes a proper pathoclinical entity in epilepsy. Using two-

photon or one-photon widefield imaging (hippocampus, neocortex), field potential and

single unit recordings, and behavioral assessment in mice, we first studied seizures

during viral encephalitis, and subsequently established an optogenetic approach to

dissociate hippocampal seizures and SD. We find profound region-specific differences in

sSD occurrence, characterize its progression, and show that temporomesial SD triggers

post-ictal wandering. Then, by Behnke-Fried (BF) electrode recordings in an initial cohort

of four patients with refractory focal epilepsy undergoing pre-surgical diagnostic work-up,

we provide corroborating evidence that region-specific sSD exists in human focal epilepsy

too, with a strikingly similar regional propensity distribution of occurrence as observed in

our murine models.

Results

Two-photon Ca^{2+} imaging of epileptic network dynamics during viral encephalitis

We initially set out to study naturally occurring temporal lobe Sz at cellular scale. To this

end, we employed resonant two-photon (2p) population Ca^{2+} imaging in the hippocampus

(CA1) or cortex (CTX, motor) of awake adult transgenic Thy1-GCaMP6s mice (JAX

025776; 15 Hz scanning, ~700x700 µm, 16X Nikon 0.80 NA 3.0 mm WD) (Fig. 1 A, B),

in the recent Theiler's murine encephalomyelitis virus (TMEV) etiocopy mouse model of

TLE. The model is based on an initial self-limiting viral encephalitis that encompasses

acute disease stage focal onset seizures (~2-7 days post infection [p.i.], Fig. 1 C, Suppl.

Fig. 1, for model details, see methods)[53].

For electrophysiological reference of optically recorded network dynamics, we combined

2p-imaging with local field potential (LFP) recordings (Fig. 1 A, insulated tungsten Ø ~125

µm). Notably, both in bi-hippocampal wireless LFP recordings in encephalitic mice (Suppl.

Fig. 2) and all combined imaging-LFP recordings in CA1 (Fig. 1 E), focal electrographic

Sz were faithfully detected bilaterally. Thus, for practical reasons, in experiments involving

both chronic in vivo 2p-imaging and LFP recordings, we placed one LFP electrode at the

stereotaxic site of hippocampal TMEV inoculation (from Bregma: AP 1.9, ML 1.6, DV 1.5

mm from pial surface), while imaging was performed in contralateral CA1 or CTX (Fig. 1

A, E). In our framework, electrographic and optical hippocampal Sz corresponded well,

while neocortical Sz invasion occurred with a delay of seconds (Fig. 1 E).

Fig. 1. Chronic hippocampal or neocortical 2p-imaging of seizures during viral encephalitis
A, Exp. setup. Contralateral (contra) cranial window above hippocampus (i: CA1) or neocortex (ii: CTX) to ipsilateral (ipsi) LFP electrode (black pin, at CA1) and TMEV injection site (CA1), in transgenic GCaMP6s mice. **B**, Exp. workflow. **C**, Detected clinical seizures (Sz, filled circles) during viral encephalitis in initial video-monitoring (7 mice, gray shades). Max. number (#) of Sz (k.d.e.: kernel density estimate) typically occur on day 2-5 post injection (d.p.i.). **D**, Representative average (avg) fluorescence (F) images of neuronal signals during pre-ictal baseline (gray), Sz (blue) and sSD (red/violet) invasion of CA1. Dotted arrows depict travelling direction of Sz (blue) or sSD (red). **E**, LFP (black, ipsi CA1) and avg population Ca²⁺ signals (green, contra) in CA1 (top) or CTX (bottom) during local Sz and sSD invasion (a.f.u.: arbitrary fluorescent units). Colored boxes correspond to time periods for avg images in D. Note that sSD is not detected in LFP with a 0.3 Hz high-pass (HP) filter (top panel), whereas a large biphasic shift is visible in

bottom panel (0.05 Hz HP). Note also delayed optical CTX Sz invasion. **F**, All imaged Sz in CA1 (13 Sz, 4
mice, blue shades) or CTX (8 Sz, 3 mice, green shades). Note the presence or absence of sSD. Dotted
lines indicate momentary breaks between imaging sessions. **G**, Quantification of occurrence of Sz-sSD,
Sz, or SD during encephalitis in CA1 (left, Friedman test, p<0.0001) or CTX (right, Friedman test, p=0.0005),
n.d. = not detected. **H**, Comparison of Sz vs SD relative Ca^{2+} signal amplitude in CA1 (a.f.u., Δ F: Delta
Fluorescence), paired Wilcoxon test (12 Sz-sSD, 117.1 $\pm$ 32.6 [Sz] vs. 164.8 $\pm$ 43.35 [sSD], p=0.0005). **I**,
Comparison of CA1 vs CTX pre- and post-ictal minimal F (a.f.u., Δ F min), Mann-Whitney test (13 events
in CA1 vs. 8 events in CTX, 3.02 $\pm$ 3.54 vs. 1.77 $\pm$ 1.04, p=0.8044). **J**, Comparison of CA1 vs CTX F
recovery time (minutes), Mann-Whitney test (13 events in CA1 vs. 8 events in CTX, 6.531 $\pm$ 2.15 vs. 0.188
$\pm$ 0.038, p=0.0061). **K**, Observed (solid lines) standard deviations (std) of spatial trajectory angles (°) of Sz
(left) or sSD1 (right) from 3 mice (blue shades, each mouse $\geq$ 3 imaged Sz-sSD) vs corresponding shuffled
distributions from 1000 randomized datasets. Dashed lines mark respective significance threshold
(observed std <95% of all surrogate std). **L**, Left: Paradigmatic experiment with spatial Sz-sSD trajectory
map within imaged field of view (M medial, L lateral, P posterior, A anterior). Outer ring shows Sz,
intermediate ring sSD1, inner ring sSD2 trajectories (gray shades: individual events, black: mean). Shaded
areas display trajectory angle between Sz and sSD1 (light blue), or sSD1 and sSD2 (dark blue). Middle and
Right: Calculated angles (°) for each imaged Sz-sSD1 and sSD1-sSD2. One event excluded from analysis,
as immediate Sz onset was not recorded, see Fig. 1 F. **M**, Quantification of angles (°) between Sz and
sSD1 (12 events, 126.9 $\pm$ 17.87), Sz and sSD2 (11 events, 143.4 $\pm$ 10.77), and sSD1 and sSD2 (12 events,
37.23 $\pm$ 8.65), mixed effects analysis with Tukey's test (F[1.396, 13.96]=26.35; Sz-sSD1 vs. Sz-sSD2
p=0.3938, Sz-sSD1 vs. sSD1-2 p=0.0020, Sz-sSD2 vs. sSD1-2 p<0.0001). For entire fig.: Plotted error bars
represent s.e.m., all given $\pm$ denote s.e.m.. Depiction of violin plots: median (solid lines), quartiles (dotted
lines). Depiction of statistical significance: n.s. not significant, *p < 0.05, **p < 0.01, ***p < 0.001, ****p <
0.0001.

Consistent association of seizures with spreading depolarization in hippocampus

Across a total of 205 imaging hours (CA1: 118 hrs; CTX: 87 hrs) in 26 mice and 158 days

of viral encephalitis, epileptiform network activity was detected in all mice. In 7 out of

those 26 mice, we successfully captured seizures (13 Sz in CA1, 4 mice [Fig. 1 F,

blue/left], 8 Sz in CTX, 3 mice [Fig. 1 F, green/right]). Strikingly, imaged hippocampal Sz

were consistently followed by a massive second, often multiplexed wave of Ca^{2+} signal,

in what appeared to be spreading depolarization / depression (SD, Fig. 1 F, G and suppl.

movie 1)[54]. In CA1, neither Sz nor SD ever occurred alone. By contrast, in CTX either

isolated SD or Sz-related SD were never detected (Fig. 1 F, G, suppl. movie 2). As

described previously, maximum hippocampal Ca^{2+} signal amplitudes of Sz-related SD

(sSD) were consistently larger than preceding Sz (Fig. 1 H)[7]. Intriguingly, despite the clear

discrepancy of sSD occurrence in CA1 versus CTX, both territories displayed reduced

basic Ca^{2+} fluorescence post-sSD (CA1) or post-Sz (CTX) in comparison to the pre-ictal

period (Fig. 1 I). However, recovery times to pre-ictal basic Ca^{2+} fluorescence in CA1

were longer than in CTX, on the order of minutes to tens of minutes (Fig. 1 J).

Hippocampal seizures and sSD propagate in opposite directions

To evaluate potentially conserved micro-progression patterns in naturally occurring

hippocampal Sz and sSD during encephalitis, we analyzed spatiotemporal Sz and sSD

trajectories across successive events similarly to previous reports[55,56]. Based on the

recruitment timepoints of identified individual neurons for a given Sz or sSD, we

calculated interpolated linear spatial trajectories of every Sz or sSD across events in all

mice with at least three recorded events where Sz and sSD onsets were fully captured (3

mice, CA1, 3.3 ± 0.3 events SEM, Fig. 1 F). As sSD often occurred in two waves

immediately following one another, we focused on the trajectory of the first wave (sSD1).

Along the antero-posterior and medio-lateral dimension of the imaged field of view (FOV),

this resulted in a number of spatial vectors per Sz and sSD1 whose respective standard

deviations could be derived and compared to randomized surrogate distributions (for

details, see methods). In all three mice, Sz trajectories displayed significantly smaller

variability in the observed dataset than would be expected by chance (Fig. 1 K left)

suggesting repeated spatiotemporal Sz progression pathways[55–57]. The same held true

for 2 out of 3 mice with regards to sSD1 (Fig. 1 K right).

Next, we investigated the relative spatial relationship between individual Sz and

successive sSD in CA1 by calculating the angles between spatial trajectories of Sz and

sSD1, and sSD1 and sSD2 (Fig. 1 L). Unexpectedly, we found vast angles between Sz

and sSD1 trajectories (Fig. 1 L, M). Typically, Sz progressed in a medio-lateral direction

(Fig. 1 L left), while sSD1 travelled the opposite way (4 mice, 12 Sz-sSD1 events, median

angle 162.01° [range 42.1 – 177.2°]) (Fig. 1 L left/middle, M). By contrast, sSD1 and sSD2

displayed more similar spatial trajectories (Fig. 1 L right, M; 4 mice, 11 sSD1-sSD2

events, median angle 42.5° [0.1 – 100.5°]).

Together, these experiments identified a complete association of naturally occurring Sz

and sSD in CA1 during viral encephalitis, whereas this association was not found in CTX.

Regardless, both CA1 and CTX displayed reduced basic fluorescence post-sSD or post-

Sz, but the post-sSD recovery time of the neuronal network in CA1 clearly outlasted the

post-Sz recovery time in CTX. All Sz, and a majority of sSD1 showed significantly non-

random spatiotemporal progression, although strikingly, hippocampal Sz and sSD1

travelled in vastly different directions.

***Post-ictal wandering* is associated with sSD in hippocampus**

In the TMEV model, we went on to correlate the observed network dynamics to clinical

signs (semiology) related to Sz or sSD. Importantly, during 2p-imaging of focal Sz in

awake head-restrained mice, generalized tonic-clonic convulsions never occurred.

What stood out at the clinical level in encephalitis-related seizures was that the mice

regularly started locomoting upon optical sSD appearance, which then lasted for minutes

(Fig. 2 A, Suppl. Fig. 3). Matching the typical time course of SD (Fig. 1 E, J), in comparison

to the pre-ictal period, locomotion was indeed systematically increased post-sSD (pre-

ictal 5min vs. post-sSD 5min, Fig. 2 B), fitting well with so-called *post-ictal* wandering, a

prominent post-ictal symptom encountered in clinical epileptology. *Post-ictal wandering*

is most frequently observed in patients with TLE[1], and characterized by confusion and

unaware wandering around (e.g. on the street). It typically lasts for minutes, at times tens

of minutes, with potentially life-threatening consequences. Aside from locomotion time,

we also quantified the travelled distance, number of locomotion episodes or maximum

locomotion speed, all of which were increased over the 5 min post-sSD period (Fig. 2 C-

E). Thus, these experiments showed that during viral encephalitis, hippocampal sSD is

associated with the onset of a locomotor phenotype that lasts for minutes, providing a

candidate mechanism for the clinical symptom *post-ictal wandering*.

Fig. 2. Hippocampal SD triggers increased locomotion
A, Locomotion on linear treadmill across 13 Sz-sSD events in all 4 CA1-imaged mice (gray shades) during encephalitis, aligned by optical Sz invasion (dotted green line), sSD onsets marked in light green. **B-E**: Comparison of 21 pre- vs. post-ictal periods (5min each) in all imaged 7 mice. **B**, % time locomotion, paired t-test (df=20; 2.525 ± 0.957 [pre] vs. 11.06 ± 2.83 [post], p=0.0059). **C**, Travelled distance (a.u.: arbitrary units), paired t-test (df=20; 1.055 ± 0.387 [pre] vs. 4.03 ± 0.915 [post], p=0.0041). **D**, # of locomotion episodes, paired t-test (df=20; 1.429 ± 0.519 [pre] vs. 4.0 ± 0.974 [post], p=0.012). **E**, maximum speed (a.u.), paired t-test (df=20; 0.312 ± 0.077 [pre] vs. 0.553 ± 0.11 [post], p=0.0523). **F**, Optogenetic experimental setup. Left (2p/1p/LFP approach): CA1 window for 2p imaging (GCaMP6s or jRGECO1a) and 1p optogenetic stimulation (ChR2), both contralateral to LFP electrode (black pin, at CA1). Right (1p/LFP approach): uni-/bilateral optogenetic stimulation (ChR2) via optical cannulae (CA1) and LFP electrode (black pin, at CA1). **G**, Co-expression of GCaMP6s (transgenic, green) and ChR2 (AAV, magenta) in CA1 (str. pyr.). **H**, Two examples for 2p/1p/LFP approach, Left: 0.75 sec optogenetic stimulation (488 nm) elicits Sz-sSD (optical ipsilateral, electrographic contralateral). Top trace depicts avg pop. Ca²⁺ signal, middle traces LFP (0.01 / 0.5 HP filter) and corresponding spectrogram, bottom trace locomotion; locomotion artifacts in LFP are marked gray in LFP traces; Right: same setting, but 4 sec optogenetic stimulation

triggers isolated SD in imaged field of view. In contralat. LFP, neither Sz nor SD are detected. Locomotion
artefacts marked in gray in LFP traces. **I**, Ratio of detectable neurons in imaged FOV (CA1) across pre-
and post-ictal periods (5min each) in 5 mice, pooled sample #: 12 ctr stim. [561/590nm], 15 SD, 9 Sz-sSD,
pre/post ratio: 1.006 ± 0.0396 (ctr), 0.433 ± 0.046 (SD), 49.33 ± 0.083 (Sz-sSD). One-way ANOVA with
Tukey's test (F [2, 33] = 35.37; ctr vs SD p<0.0001, ctr vs Sz-sSD p<0.0001, SD vs. Sz-sSD p=0.7265. **J**,
Optogenetic stim. framework for analysis in K to N. **K-N**, Comparison of respective value Δ between pre-
and post-ictal periods (5min each) in 7 mice (2p/1p/LFP or 1p/LFP approach), pooled sample #: 33 ctr stim.,
17 unilateral SD, 20 Sz-sSD, 10 bilateral SD. **K**, Δ % time locomotion: -4,403 ± 1.187 (ctr), 8.331 ± 1.861
(unilat. SD), 32.18 ± 3.540 (Sz-sSD), 40.68 ± 4.325 (bilat. SD). One-way ANOVA with Tukey's test
(F[3,76]=72.44; ctr vs unilat. SD p=0.001, ctr vs Sz-sSD p<0.0001, ctr vs. bilat. SD p<0.0001, unilat. SD vs.
Sz-sSD p<0.0001, unilat. SD vs. bilat. SD p<0.0001, Sz-sSD vs. bilat. SD p=0.1862). **L**, Δ travelled distance
(a.u.): -1.805 ± 0.591 (ctr), 5.027 ± 1.063 (unilat. SD), 22.80 ± 2.713 (Sz-sSD), 25.95 ± 3.195 (bilat. SD).
One-way ANOVA with Tukey's test (F[3, 76]=62.57; ctr vs unilat. SD p=0.0178, ctr vs Sz-sSD p<0.0001,
ctr vs. bilat. SD p<0.0001, unilat. SD vs. Sz-sSD p<0.0001, unilat. SD vs. bilat. SD p<0.0001, Sz-sSD vs.
bilat. SD p=0.7077). **M**, Δ # of locomotion episodes: -1.697 ± 0.4636 (ctr), 4.176 ± 1.129 (unilat. SD), 8.05
± 0.95 (Sz-sSD), 7.0 ± 1.461 (bilat. SD). One-way ANOVA with Tukey's test (F[3, 76]=32.48; ctr vs unilat.
SD p<0.0001, ctr vs Sz-sSD p<0.0001, ctr vs. bilat. SD p<0.0001, unilat. SD vs. Sz-sSD p=0.0152, unilat.
SD vs. bilat. SD p=0.2561, Sz-sSD vs. bilat. SD p=0.8929). **N**, Δ maximum speed (a.u.): -0.1516 ± 0.0523
(ctr), 0.072 ± 0.063 (unilat. SD), 0.243 ± 0.077 (Sz-sSD), 0.366 ± 0.106 (bilat. SD). One-way ANOVA with
Tukey's test (F[3, 76]=10.80; ctr vs unilat. SD p=0.0803, ctr vs Sz-sSD p=0.0001, ctr vs. bilat. SD p<0.0001,
unilat. SD vs. Sz-sSD p=0.3423, unilat. SD vs. bilat. SD p=0.0876, Sz-sSD vs. bilat. SD p=0.7322). For
entire fig.: All given ± denote s.e.m.. Depiction of violin plots: median (solid lines), quartiles (dotted lines).
Depiction of statistical significance: n.s. not significant, *p < 0.05, **p < 0.01, ***p < 0.001, ****p < 0.0001.
246

Optogenetic dissection of the role of hippocampal SD in *post-ictal wandering*

Although hippocampal sSD appearance coincided with the onset of sustained locomotion

during encephalitis, the complete association of hippocampal Sz and sSD precluded us

from decisively differentiating the role of Sz versus SD in *post-ictal wandering*. To arrive

at a more mechanistic understanding, based on previous studies[58,59], we established a

combined 2p-imaging (GCaMP6s [JAX 025776], or jRGECO [AAV2/1-NES-jRGECO1a]

Vector Core Uni Bonn), 1p optogenetics (ChR2, AAV-hSyn-hChR2[H134R]-mCherry,

Addgene ID 26976-AAV5) and LFP approach (Fig. 2 F left; 2 G, suppl. Fig 4) that allowed

us to generate either Sz or SD in a controlled manner. Using this 2p/1p/LFP approach,

Sz or SD were never elicited by 2p-imaging (16X Nikon 0.80 NA, wavelength range 940-

980nm [GCaMP] or 1050nm [jRGECO]).

In CA1, Sz could be reliably elicited by a brief square wave light pulse (typically 500-

750ms, Coherent Inc., CA, Sapphire LP CW laser, 488nm, power at brain surface 4-

5mW/mm^2) in the imaged FOV (Fig. 2 H). Interestingly, these optogenetically induced Sz

in the healthy hippocampus were again consistently followed by sSD, and Sz-sSD could

be bilaterally detected (Fig. 2 H left, suppl. movie 3). To reliably trigger isolated SD without

a preceding focal Sz, a prolonged light pulse (~4 sec, 488nm, 4-5mW/mm^2) was applied,

similarly to previous reports (Fig. 2 H right, suppl. Fig. 4 C, suppl. movies 4, 5)[42,43]. Neither

Sz nor SD could be elicited by control illumination at 561nm (Coherent Inc., Santa Clara,

CA, Sapphire LP CW laser, 7 mW/mm^2), ensuring that the effects were not unselectively

driven by laser light alone. Notably, a comparison of encephalitic hippocampal sSD and

optogenetic hippocampal SD with respect to optical signal amplitude, SD$_{depol}$ half-width,

and SD progression speed, showed no significant differences (suppl. Fig. 5 A-C). Thus,

basic SD features were preserved across our different Sz models. In line with our imaging

experiments during encephalitis, both optogenetically triggered Sz-sSD and isolated SD

led to an equally strong post-ictal reduction of detectable neurons in the FOV (Fig. 2 I)

underscoring functional depression of the CA1 network due to SD. To make sure that

these optical imaging results were not confounded by GFP-quenching due to SD-related

pH shifts (ongoing neuronal firing in the quenched absence of optical signals), we

repeated the optogenetic SD experiments with electrophysiology, now employing

hippocampal tetrode recordings (+ optical cannula, see methods) instead of 2p-imaging.

In keeping with the imaging experiments, we found a prolonged and profound cessation

of firing of a large majority of units upon optogenetic SD in CA1 (suppl. Fig. 5 D).

As unilateral optogenetic Sz induction consistently triggered bi-hippocampal Sz (Fig. 2 H

left), we additionally implemented a 1p optogenetic stimulation approach enabling uni- or

bilateral hippocampal Sz or SD induction via implanted optical cannulas, combined with

LFP recordings (1p/LFP approach; Fig. 2 F right). Here, for optogenetic Sz or SD

induction versus control, instead of lasers, fiber-coupled LEDs were employed using the

same stimulation durations as mentioned above (Chrolis/Thorlabs: 475 nm or 590nm [2-

3mW/mm^2]). Based on the 2p/1p/LFP or 1p/LFP approach, we then compared a pre- and

post-stimulation (for control and SD) or pre-stimulation and post-sSD (for Sz-sSD) period

(5min each, Fig. 2 J) analyzing the same locomotor parameters as in the context of

encephalitic Sz-sSD (Fig. 2 B-E).

In the initial 2p/1p/LFP experiment, we unilaterally triggered SD or Sz versus unilateral

control (Suppl. Fig. 6 A-D). In the 1p/LFP experiment, we carried out bilateral SD,

unilateral Sz (except in one animal, where bilateral stimulation was necessary to trigger

hippocampal Sz), and uni- or bilateral control stimulations (Suppl. Fig. 6 E-H). Since with

respect to all analyzed clinical parameters, uni- versus bilateral control stimulations

showed no significant differences, neither within the 1p/LFP configuration (Suppl. Fig. 6

E-H) nor across experimental configurations (Suppl. Fig. 6 I-L), these data were pooled.

As the same held true for uni- and bilateral hippocampal Sz inductions within and across

experiments, these data were also pooled (Suppl. Fig. 6 I-L, statistics for suppl. Fig. 6 are

displayed in suppl. Table 1 and 2).

Remarkably, in comparison to control, isolated optogenetic unilateral SD in CA1 was

sufficient to reproduce the locomotor phenotype that we had observed upon Sz-sSD in

CA1 during encephalitis, proving that hippocampal SD alone is sufficient to trigger *post-*

ictal wandering (Fig. 2 K-N, suppl. Fig. 7). Interestingly, across most tested locomotor

parameters (% time of locomotion, travelled distance, number of locomotion episodes),

the effect triggered by unilateral hippocampal optogenetic SD stimulation was significantly

surpassed by unilateral hippocampal optogenetic Sz-sSD stimulation (Fig. 2 K-N, suppl.

Fig. 7). We hypothesized that this difference in effect size could be due to the bilateral

hippocampal involvement during focal onset hippocampal seizures, which we had

observed during encephalitis and optogenetic experiments (Fig. 1 E, 2 H left). In this case,

even a unilaterally triggered hippocampal Sz would, due to its bi-hippocampal

recruitment, lead to bilateral hippocampal sSD (Fig. 2 H left). In turn, unlike hippocampal

Sz-sSD, due to the different, non-synaptic nearest-neighbor progression of SD,

unilaterally triggered SD would typically remain unilateral (Fig. 2 H right). In line with this

rationale, uni- or bilateral hippocampal Sz-sSD stimulation produced a similar locomotor

phenotype (Suppl. Fig. 6 E-H), and Sz-sSD stimulation systematically produced a

stronger phenotype as compared to unilateral optogenetic SD stimulation, except for

maximum speed (Fig. 2 K-N, suppl. Fig. 6 A-D and I-L). Yet crucially, Sz-sSD and bilateral

SD stimulation consistently evoked a similar clinical phenotype across analyzed

locomotor parameters (Fig. 2 K-N, suppl. Fig. 6 E-L, suppl. Fig. 7). Together, these

experiments unveiled i) a mechanistic role of hippocampal SD in *post-ictal wandering*, ii)

a scaling of severity of the clinical phenotype depending on uni- versus bilateral

hippocampal SD, and iii) similar clinical effect sizes across hippocampal Sz-sSD and

bilateral SD. Therefore, rather than Sz themselves, these experiments point towards a

role of hippocampal SD in *post-ictal wandering*.

Optogenetic induction of hippocampal SD and neocortical widefield imaging

While we had never observed Sz-sSD in motor cortex using 2p-imaging during encephalitis, our imaged FOV was confined to ~700x700 µm. Thus next, with the optogenetic approach of on-demand focal SD induction at hand, and combined LFP recordings and one-photon (1p) widefield Ca^{2+} imaging, we went on to investigate the potential spread of optogenetic unilateral hippocampal SD to CTX[28,29]. For hemispheric neocortical 1p-imaging (30 Hz scanning, 470 / 405 nm, LED M470L3 / M405L3, Thorlabs) through cleared skull in awake adult mice, we employed an inverted tandem lens macroscope[60], and transgenic tetO-GCaMP6s / CaMK2a-tTA mice (JAX 024742 / 007004) expressing GCaMP6s in excitatory neurons across all cortical layers (for details, see methods) (Fig. 3 A).

Fig. 3. Hippocampal SD coactivates but does not invade neocortex
A, Top: Experimental setup, widefield Ca^{2+} imaging of neocortex (CTX) in tetO-GCaMP6s/CaMK2a-tTA mice through cleared skull, in combination with hippocampal optogenetic 1p stimulation (ChR2, optical cannula at CA1) and LFP (black pin, at CA1), Bottom: Example image of cortical surface after skull clearing, and implant sites of LFP electrode (white filled circle) and optical fiber (blue circle). Overlaid white lines show Allen CCF borders. **B**, Two examples of stimulus-related CTX activity. Hippocampal (HPC) LFP of

optogenetic SD stimulation (5 sec, blue line), and cortical widefield Ca^{2+} activity in secondary/primary motor
(M2, M1) and parietal cortex (P). Corresponding to pre- (orange) and post-stim. periods (violet) 10-sec avg
Δ F/F images of CTX activity (bottom, white circles depict M2, M1, P). Note immediate post-stim. widefield
CTX activation and continued post-stim. activity, either without any baseline F shift (left) or a brief transient
negative baseline shift (right), yet always with continued presence of cortical Ca^{2+} transients. **C**,
Superposition of peri-stim. CTX Δ F/F activity traces (individual traces in gray, mean in black; 3 mice, 12
HPC SD stim. [4/mouse, 1/day]). **D**, Quantification of pre- (-10 - 0 sec to stim., orange) vs. post-stim. (0 –
10 sec from stim., violet) avg CTX activity in M2 (0.01 $\pm$ 0.252 [pre] vs. 1.589 $\pm$ 0.337 [post]), M1 (0.118 $\pm$
0.348 [pre] vs. 1.778 $\pm$ 0.371 [post]) and P (-0.044 $\pm$ 0.196 [pre] vs. 1.831 $\pm$ 0.432 [post]). One-way ANOVA
with Šidák's test (F[2.146, 23.60] = 17.98; pre vs. post: M2 p=0.0029, M1 p=0.0014, P p=0.0018). No
significant differences of Δ (post – pre) activity among M2, M1, and P. One-way ANOVA with Tukey's test
(F[1.837, 20.21]=0.5231; M2 vs. M1 p=0.946, M2 vs. P p=0.657, M1 vs. P p=0.766). **E**, Cross-correlation
of peri-stim. activity of M2 and P (12 HPC SD stim., [4/mouse, 1/day], individual traces in gray, mean in
black), mean lag = 0 sec. **F**, Pre- and post-ictal (5min each) activity correlation of M2, M1, and P. Note
increased correlation of activity over 5min post HPC SD stimulation. **G**, CTX pre- vs. post-ictal minimal F
(Δ min F baseline/min F post-ictal; M2 0.739 $\pm$ 0.243, M1 0.781 $\pm$ 0.26, P 0.643 $\pm$ 0.247), One-way ANOVA
with Tukey's test (F[2, 33]=0.0807; M2 vs. M1 p=0.992, M2 vs. P p=0.96, M1 vs. P p=0.919). Note that all
areas show a decreased post-stim. min F on avg. **H**, Comparison of cross-area F recovery time (sec, M2
18.33 $\pm$ 4.323, M1 19.58 $\pm$ 4.15, P 22.5 $\pm$ 5.418), One-way ANOVA with Tukey's test (F[2, 33]=0.2102; M2
vs. M1 p=0.98, M2 vs. P p=0.804, M1 vs. P p=0.898). For entire fig.: All given $\pm$ denote s.e.m.. Depiction of
violin plots: median (solid lines), quartiles (dotted lines). Depiction of statistical significance: n.s. not
significant, *p < 0.05, **p < 0.01, ***p < 0.001, ****p < 0.0001.
366

Around six weeks before the actual experiment, pAAV-hSyn-hChR2(H134R)-mCherry

was stereotactically injected into the left hippocampal CA1 region (coordinates from

Bregma: AP -1.9, ML -1.6, DV -1.5 mm). In addition, a custom-made optrode comprising

an insulated tungsten electrode (Ø ~125 μm) and an optical fiber (Ø 200 μm, NA = 0.37)

were chronically implanted above the left hippocampus, for LFP recordings and optical

stimulation.

Similar to our previous optogenetic experiments, hippocampal SD could be reliably

induced by a square wave light pulse (5 sec, 488 nm, 15 mW/mm^2, 1p CW laser

READYBeam™ Bio2, FISBA AG, SUI) (Fig. 3 B). For practical procedural reasons related

to the optrode implant, imaging was carried out in the cortical hemisphere contralateral to

hippocampal SD induction (Fig. 3 A). While a widespread coactivation of CTX (e.g. motor

cortex: M2, M1; parietal cortex: P) was observed during optogenetically induced

hippocampal SD across 12 recordings (4 mice, 3 SD each, one SD stim/d, Fig. 3 B-D),

no SD or wave-like invasion resembling SD dynamics were ever observed in CTX.

Moreover, no activation lags could be found across distant neocortical areas (e.g. M2/P,

Fig. 3 E), and CTX continued to show typical transients of Ca^{2+} activity (Fig. 3 B). Notably,

neocortical areas showed an enhanced correlation of activity in the post-stimulation

period (Fig. 3 F). Still, similar to our 2p-imaging results in CTX during encephalitis, cortical

dynamics across regions also often displayed, although moderately, a reduction of basic

fluorescence in the immediate post-stimulation period despite the absence of SD (Fig. 3

B right, 3 C and G, suppl. Fig. 8). Importantly, also during this time, Ca^{2+} transients

continued without interruption (Fig. 3 B right). Further, as in our 2p-imaging experiments,

the recovery to pre-stimulation basic fluorescence was consistently fast in CTX (<1 min,

Fig. 3 H). Together, these experiments recapitulated results from our 2p-imaging

experiments, and corroborated the evidence that hippocampal SD typically does not

propagate to CTX. Moreover, neocortical Ca^{2+} transients appeared to continue

throughout the post-stimulation period without signs for activity depression, and, in

contrast to SD dynamics, showed a rapid recovery from reduced basic fluorescence to

pre-stimulation conditions.

Seizure-related focal SD in human epilepsy

The current EEG-standard with a bandwidth of 0.5-70 Hz[61] renders SD invisible in clinical

practice. While SD related to spontaneous Sz has been documented in rodent epilepsy

models[29], it is not known whether it occurs in human epilepsy. Thus, we finally sought to

examine the existence, and potentially regional preference of sSD in human focal

epilepsy through multi-regional Behnke-Fried (BF) electrode recordings, in the context of

stereotactic depth macro-electrode recordings (SEEG) during pre-epilepsy-surgery

diagnostic work-up (Fig. 4 A, B, see methods for details).

Fig. 4. Focal Sz-sSD occurs in human epilepsy
406
A, Scheme and dimensions of individual Behnke-Fried (BF) electrodes composed of depth-electrode
macro-contacts and microwire bundle. **B**, 3D-reconstructed brain MRI and location of implanted BF
electrodes. Green dots indicate macro-contact locations, shades of green designate different brain regions

and violet markers depict microwire bundles. AMD: amygdala, aHPC: anterior hippocampus, EC: entorhinal
cortex, pHPC: posterior hippocampus, PHC: parahippocampal cortex, PIC: piriform cortex, Ta: temporal
cortex a, Tb: temporal cortex b. **C i**, LFP traces from BF microwire bundles across recorded regions (0.1
HP filter, referenced to local common average) of a temporomesial focal onset Sz. **C ii**, magnified inset
from Ci, aHPC (as marked by orange lines). Note slow LFP shift at the end of Sz, confined to HPC. **D**,
Regional occurrence count of sSD across all Sz-invaded regions (all Sz/patients included). **E**, aHPC, most
distal macro contact trace (top), corresponding microwire trace (middle) and multi-unit activity from the
same microwire (bottom). **F**, Change in power between the first postictal minute and the preictal minute.
Each line represents one Sz-invaded microwire, color shades indicate Sz-invaded (gray, sSD-neg.) and
Sz-sSD-invaded (purple, sSD-pos.) regions, bold lines depict the mean of each group. **G**, Comparison of
respective Δ pre- and post-ictal broadband power (dB, 2-50 Hz) in sSD-neg. (18 events) vs. sSD-pos. (5
events) Sz-invaded regions, unpaired t-test (-1.365 ± 0.8728 [sSD-neg.] vs. -5.870 ± 1.107 [sSD-pos.],
p=0.0189). **H**, Comparison of postictal broadband power recovery time (min) of sSD-neg. (18 events) vs.
sSD-pos. (5 events) Sz-invaded regions, Mann-Whitney test (16.7 ± 3.84 [sSD-neg.] vs. 84.87 ± 51.29
[sSD-pos.], p=0.0112). **I**, Comparison of respective Δ pre- and post-ictal high-gamma power (dB, 80-150
Hz) in sSD-neg. (18 events) vs. sSD-pos. (5 events) Sz-invaded regions, unpaired t-test (-1.184 ± 0.544
[sSD-neg.] vs. -4.227 ± 0.6825 [sSD-pos.], p=0.0117). **J**, Comparison of postictal high-gamma power
recovery time (min) of sSD-neg. (18 events) vs. sSD-pos. (5 events) Sz-invaded regions, Mann-Whitney
test (27.05 ± 11.00 [sSD-neg.] vs. 37.97 ± 7.08 [sSD-pos.], p=0.078). For entire fig.: All given ± denote
s.e.m.. Depiction of violin plots: median (solid lines), quartiles (dotted lines). Depiction of statistical
significance: n.s. not significant, *p < 0.05, **p < 0.01.
431

As an initial cohort, we included four patients (2 female / 2 male patients, age range 23-

50 yrs) with refractory focal epilepsy based on different pathologies, a history of post-ictal

symptoms comprising post-ictal wandering, aphasia or confusion, and depth electrodes

in the temporal lobe (Fig. 4 B, for implant schemes and clinical information, see suppl.

Fig. 9). Across a total of 272 BF microelectrodes (8/bundle), 7 brain regions (amygdala,

hippocampus [ant., post.], entorhinal / parahippocampal / piriform / temporal cortex), and

39 recording days during pre-surgical evaluation, 16 focal-onset seizures were recorded.

Strikingly, we found what appeared to be highly localized sSD in the BF microwire

recordings (Fig. 4 Ci, Cii) in every patient (4/16 Sz in total). In the per-region analysis of

Sz-invasions, in line with our murine recordings, we found sSD to occur primarily in

temporomesial regions, while it was not detected in the other recorded regions (Fig. 4 C,

D). At the same time, sSD was not visible at the clinical macroelectrodes (Fig. 4 E, top

panel). On average, both non-sSD and sSD regions displayed a postictal/post-sSD

reduction in spectral power (Fig. 4 F), but sSD regions showed a more profound decrease,

and a delayed recovery to the pre-ictal condition (Fig. 4 G, H). Consistent with our murine

results and previous literature[8,17,32,62], at the neuronal unit level, sSD invasion coincided

with a break-down of neuronal firing (Fig. 4 E, middle and bottom panel). To compare

neuronal activity independently of stably trackable neuronal units, we used high gamma

(80-150 Hz) oscillatory power as a proxy, as previously described[63]. Again, on average,

both sSD-neg. and sSD-pos. regions showed a decreased post-ictal high gamma power,

but sSD-pos. regions displayed a stronger reduction, and delayed recovery (Fig. 4 I, J).

In sum, these recordings unveiled that focal sSD exists in human focal epilepsy, and

suggest an increased propensity of temporomesial regions to experience sSD across a

cohort of 4 patients. Further, among Sz-invaded areas, sSD-pos. regions take longer to

recover to their pre-ictal baseline in comparison to sSD-neg. regions.

Discussion

This work suggests that seizure-associated focal spreading depolarization (sSD) is a

pathoclinical hallmark of epilepsy. We find profound region-specific differences in sSD

occurrence, characterize its progression, and show that temporomesial SD causes post-

ictal wandering. Then, in a cohort of 4 human epilepsy patients with BF electrode

recordings, we show that sSD exists in human focal epilepsy. In this cohort, sSD

displayed a similar temporomesial propensity as in our murine experimental models.

While we observed sSD primarily in temporomesial structures in both mice and humans,

several aspects require discussion in this regard. First, our analyses were based on focal

onset seizures with known or suspected origin in the temporal lobe, with known or

suspected seizure onset zones (SOZ) situated there too. Therefore, sSD emergence may

simply depend on its spatial relationship to SOZ and (peri-)lesional tissue. Still, there are

basic neuroanatomical features that inherently predispose e.g. the hippocampus to sSD.

First, hippocampal wiring with itself and other regions renders it more excitable than other

portions of the brain such as the neocortex[64,65]. In line with this longstanding notion, our

hippocampal optogenetic Sz-induction protocol failed to induce seizures in healthy

neocortex. At the synaptic level, the CA3 region contains so-called "conditional detonator"

synapses that can strongly drive postsynaptic firing[66], which may be why CA3 displayed

a high propensity for SD upon repetitive mossy fiber stimulation under hyperexcitable

conditions[67]. Further, aside from its neuronal connectivity, recent data suggests that the

hippocampus displays relatively reduced blood oxygenation and neurovascular coupling

in comparison to neocortex due to differences in vascular architecture[68]. Among other

potential contributing factors such as subregion-specific oxidative metabolic capacity[69],

this may make the hippocampus susceptible to an energy shortage during seizures,

promoting sSD. We propose that in addition to possible (peri-)lesional vulnerabilities for

sSD, basic neuroanatomical differences across brain regions support differential sSD

occurrence rates. This carries implications for notions revolving around regional post-ictal

EEG signal depression and its spatial overlap with the assumed SOZ[70]. It is possible that

e.g. the hippocampus, even if only secondarily recruited into a Sz, may be at risk for sSD

due to its anatomy. This could then prompt post-ictal signal depression in this territory

without it being part of the SOZ.

Adhering to the neuroanatomical argument, regarding the disparate spatiotemporal

trajectories of Sz and sSD in our imaging experiments, work by Scharfman on SD

susceptibilities of hippocampal sub-regions[67] may provide a potential explanation for this

unexpected result. We always imaged CA1 contralateral to the TMEV CA1 injection site,

and consistently observed a mediolateral Sz spread. sSD mostly travelled the other way,

which points towards CA2 or CA3 as the source of sSD[67]. Based on Scharfman's dual

region electrical recordings, her observation that mossy-fiber-stimulation-triggered SD in

CA3 travelled back to dentate gyrus (DG)[67], and our CA1 imaging results, one could

hypothesize that CA3-prompted sSD propagate both towards DG and CA1. Alternatively,

CA2 could be an sSD source, as it receives strong excitatory input from entorhinal cortex,

and has been shown to display enhanced excitability in chronic epilepsy[71,72]. Finally, it is

also conceivable that multiple potential sSD generators exist across CA regions.

A main finding of this study is that hippocampal SD triggers post-ictal wandering.

Importantly, this does not *per se* mean that the hippocampus is the primary driver of the

observed phenotype. While a transient shutdown of hippocampal networks will contribute

to unaware post-ictal wandering e.g. through navigational confusion, it is likely that the

enhanced locomotion upon hippocampal SD is brought about by a number of

interconnected brain regions[73,74] that interact with the hippocampus and that may be

indirectly or directly affected by hippocampal SD, including the septum[75,76] and

mesencephalic structures[73,77]. Clearly also, while in our murine models, sSD was

observed only in hippocampus during viral encephalitis, and optogenetic hippocampal SD

did not invade neocortex, this does not mean that it never does (it can, see [28,29]), nor that

it does not invade other subcortical structures (we hypothesize that it does), nor that it

does not invade the hippocampus if emerging elsewhere (e.g. in the neocortex[28]).

At a wider scope, this works carries implications for epilepsy research and neurology.

Surely, while much has been learned about SD in neurological research e.g. on migraine

or traumatic brain injury[10–12], the relationship between SD and clinical symptoms in

epilepsy has remained understudied. Part of the reason is that most studies on SD in

epilepsy have been carried out in vitro, or under anesthesia[8,9,23,26,49,50], which precludes

clinical correlation. At other times, it was not primarily intended to link neurophysiological

measures to clinical semiology, i.e. in studies focusing on SD-related Sz termination[50,51].

Most epilepsy research studies do not specifically distinguish Sz with or without SD,

although SD has long been suggested to represent a 'separate entity' (see Bureš et al.[24],

p.10). Based on this suggestion and the results shown here, it may indeed be the case

that some of the previously observed effects attributed directly to Sz are instead mediated

by sSD. Notably, as Sz and sSD can co-occur at the same time in different brain regions,

this also extends to clinical semiology. Some previously described "ictal" symptoms may

present compound semiology based on spatially separate, simultaneous Sz and sSD.

Re-visiting reported effects and effect-sizes, and clinical symptoms through the lens of

Sz versus sSD will likely propel new diagnostic and therapeutic research on many acute

and chronic clinical circumstances that involve seizures, and thus potentially, sSD.

Due to the current clinical EEG standard (>0.5 Hz)[61], SD is invisible in routine clinical

care. As a result, medical professionals regularly encounter post-ictal symptoms, but are

blind to SD as a potential major determinant of these phenomena. As there is a

traditionally strong focus on the "ictus" in epileptology (highlighted by current terminology),

such symptoms are then usually related to Sz, and sSD plays little to no role in the clinical

framework. Inversely, it is known in basic research that sSD terminates ongoing Sz[27,50],

but since SD-mediated Sz termination have been studied mostly in vitro or under

anesthesia, the clinical impact of sSD could not be studied. Thus, our results underscore

the necessity of a close cross-talk between clinical and basic research disciplines.

Clearly, sSD can have potentially life-threatening clinical consequences[4,5]. In our view,

caution is required if sSD is proposed as a protective factor of the brain against seizures,

and as a potential epilepsy treatment tool[50,52]. Rather, our work supports the notion that

SD constitutes a transient homeostatic break-down of a biological system driven beyond

its physiological range of operation[32].

There are of course limitations to this study. First, although our murine findings held true

across recording modalities, two different murine models of hippocampal Sz and SD, and

under healthy (optogenetics) and disease (TMEV) conditions, we do not know whether

these findings extend across many different etiologies. Aside from the factors discussed

above, the exact parameters that favor sSD emergence in hippocampal Sz are not yet

clear, and may include e.g. Sz duration, extent of spatial Sz invasion and hippocampal

subfields, Sz dynamics (e.g. tonic vs. clonic), internal state or transition between states

(e.g. wakefulness, sleep). Further, there are limitations related to the human data included

in this study. In our wide-bandwidth AC recordings, the lowest possible high-pass filter

was 0.1 Hz for technical reasons. Therefore, it is possible that some sSDs were missed,

and if anything, the true occurrence rate may be higher. Another reason for a possible

underestimation of the true sSD occurrence rate is that current depth electrode recordings

strongly spatially undersample targeted brain areas. In the near future this limitation may

become softened to some extent, on the heels of recent advances in high-density

electrode arrays[78–81]. First steps towards a systematic investigation of sSD in larger

patient cohorts will require coordinated efforts by institutions that have access to wide-

bandwidth AC or DC-coupled intracranial electrical recordings in epilepsy patients.

Beyond the currently available recording modalities in clinical practice, one should

consider newly available technology for potential high-fidelity full-bandwidth recordings of

Sz, SD and sSD in humans, e.g. biocompatible flexible microtransistors[28].

In sum, this work sets stage for a wider discussion of the pathoclinical role of sSD in

epilepsy, and a potential re-consideration of the clinical EEG filter standard[61]. Beyond

post-ictal wandering, our results suggest that focal sSD could underlie other post-ictal

symptoms, e.g. confusion, receptive aphasia, navigational impairment, or defensive-like

aggression[3,82,83]. Finally, it seems plausible that sSD does not only trigger immediate

post-ictal symptoms, but also exerts chronic effects, e.g. on cognitive function. Thus, it

may play a role in comorbidities of epilepsy, and other diseases encompassing temporal

lobe pathology and seizures, e.g. neurodegenerative diseases, which are not primarily

treated by epileptologists.

Acknowledgements. We sincerely thank Lea Adenauer for outstanding technical
support, and Negar Nikbakth, Nicola Masala, and Martin Pofahl for their technical advice.
We appreciate Lisa Rottenfußer's support and input during her M.Sc. lab rotation.
Generally, we are grateful to members of the Wenzel, Beck, Ewell, and Mormann
laboratories for comments. This work was supported by the BONFOR Program at
University of Bonn (M.W.: #2019-2-04), the Hertie Network of Excellence in Clinical
Neuroscience (M.W.: #P1200008), and the German Research Foundation (DFG;
SFB1089 to M.W., L.E., H.B., and #504342801 to M.W.). The work was further supported
by the iBehave network (M.W., S.M., H.B.), the Helmholtz association (S.M.: VH-NG-
1611), and the European Research Council (M.W.: StG #101039945). We also
acknowledge the support of the Viral Vector Service Core Facility, and the Imaging Core
Facility of the Bonn Technology Campus Life Sciences funded by the Deutsche
Forschungsgemeinschaft (DFG, German Research Foundation, project #388169927).
598

Author contributions. M.W. conceived the project. M.W. and B.M. wrote the paper with
input from all authors. Experimental contributions: Multimodal 2-photon imaging
experiments: B.M., M.W., M.K., M.B., T.T., T.O.. Multimodal 1-photon imaging
experiments: N.B., S.M.. Tetrode recordings: A.N.H., M.K.. Wireless LFP recordings:
A.B., J.P., M.W.. Optogenetics (combined with imaging/electrophysiology, via cranial
window/cannulas): M.K., M.W., B.M., T.T., A.N.H., N.B., S.M.. Immunohistochemistry and
confocal microscopy: L.K., M.B., Š.G., M.S-S., A.B., J.P.. TMEV was produced and
provided by I.G. and W.B.. All data processing and analyses were carried out by B.M.
and M.W., except: Multimodal 1-photon imaging experiments: S.M., N.B., M.W.. Tetrode
recordings: A.N.H., L.E., A.G.G., M.K.. Immunohistochemistry and confocal microscopy:
L.K., M.B., Š.G., M.S-S., A.B., J.P.. Processing and analysis of human recordings:
A.G,G., M.W., F.M.. H.B., R.S., and F.M. provided infrastructure, experimental, analytical,
and clinical expertise.

Materials & Correspondence. Correspondence and material requests should be
addressed to michael.wenzel@ukbonn.de

References

1.   Tai, P. *et al.* Postictal wandering is common after temporal lobe seizures. *Neurology* **74**,

932–933 (2010).

2.   Grant, A. C., Koziorynska, E., Lushbough, C., Maus, D. & Mortati, K. Acute postictal

confusion and violence: Two cases with unfortunate outcomes. *Epilepsy Behav. Case*

Reports **1**, 71–73 (2013).

3.   Pottkämper, J. C. M., Hofmeijer, J., van Waarde, J. A. & van Putten, M. J. A. M. The

postictal state — What do we know? *Epilepsia* **61**, 1045–1061 (2020).

4.   Aiba, I. & Noebels, J. L. Spreading depolarization in the brainstem mediates sudden

cardiorespiratory arrest in mouse SUDEP models. *Sci. Transl. Med.* **7**, (2015).

5.   Loonen, I. C. M. *et al.* Brainstem spreading depolarization and cortical dynamics during

fatal seizures in Cacna1a S218L mice. *Brain* **142**, 412–425 (2019).

6.   Farrell, J. S. *et al.* Postictal behavioural impairments are due to a severe prolonged

hypoperfusion/hypoxia event that is COX-2 dependent. *Elife* **5**, 1–24 (2016).

7.   Farrell, J. S. *et al.* In vivo assessment of mechanisms underlying the neurovascular basis

of postictal amnesia. *Sci. Rep.* **10**, 1–13 (2020).

8.   Leao, A. A. P. Spreading Depression of Activity in the Cerebral Cortex. *J. Neurophysiol.*

7, 359–390 (1944).

9.   Takano, T. *et al.* Cortical spreading depression causes and coincides with tissue hypoxia.

Nat. Neurosci. **10**, 754–762 (2007).

10.   Lemale, C. L. *et al.* Migraine Aura, Transient Ischemic Attacks, Stroke, and Dying of the

Brain Share the Same Key Pathophysiological Process in Neurons Driven by Gibbs–

Donnan Forces, Namely Spreading Depolarization. *Front. Cell. Neurosci.* **16**, 1–29

(2022).

11.   Cozzolino, O. *et al.* Understanding spreading depression from headache to sudden

unexpected death. *Front. Neurol.* **9**, 1–13 (2018).

12.   Dreier, J. P. The role of spreading depression, spreading depolarization and spreading

ischemia in neurological disease. *Nat. Med.* **17**, 439–447 (2011).

13.   Bosche, B. *et al.* Recurrent spreading depolarizations after subarachnoid hemorrhage

decreases oxygen availability in human cerebral cortex. *Ann. Neurol.* (2010).

doi:10.1002/ana.21943

14.   Hartings, J. A. *et al.* Prognostic Value of Spreading Depolarizations in Patients with

Severe Traumatic Brain Injury. *JAMA Neurol.* **77**, 489–499 (2020).

15.   Dreier, J. P. *et al.* Spreading convulsions, spreading depolarization and epileptogenesis

in human cerebral cortex. *Brain* **135**, 259–275 (2012).

16.   Dohmen, C. *et al.* Spreading depolarizations occur in human ischemic stroke with high

incidence. *Ann. Neurol.* **63**, 720–728 (2008).

17.   Nasretdinov, A. *et al.* Diversity of cortical activity changes beyond depression during

Spreading Depolarizations. *Nat. Commun.* **14**, (2023).

18.   Fabricius, M. *et al.* Association of seizures with cortical spreading depression and peri-

infarct depolarisations in the acutely injured human brain. *Clin. Neurophysiol.* **119**, 1973–

1984 (2008).

19.   Strong, A. J. *et al.* Spreading and synchronous depressions of cortical activity in acutely

injured human brain. *Stroke* **33**, 2738–2743 (2002).

20.   Mayevsky, A. *et al.* Cortical spreading depression recorded from the human brain using a

multiparametric monitoring system. *Brain Res.* **740**, 268–274 (1996).

21.   Dreier, J. P. *et al.* Delayed ischaemic neurological deficits after subarachnoid

haemorrhage are associated with clusters of spreading depolarizations. *Brain* **129**, 3224–

3237 (2006).

22.   Drenckhahn, C. *et al.* Correlates of spreading depolarization in human scalp

electroencephalography. *Brain* **135**, 853–868 (2012).

23.   Sramka, M., Brozek, G., Bures, J. & Nadvornik, P. Functional Ablation by Spreading

663   Depression: Possible Use in Human Stereotactic Neurosurgery. *Appl. Neurophysiol.* **40**,

664   48–61 (1978).

665   24.   Bureš, J., Burešová, O. & Křivánek, J. *The mechanism and applications of Leao's*

666   *spreading depression of electroencephalographic activity. ACAD.PRESS, NEW YORK,*

667   *N.Y.* (1974).

668   25.   Kunkler, P. E. & Kraig, R. P. Hippocampal spreading depression bilaterally activates the

669   caudal trigeminal nucleus in rodents. *Hippocampus* **13**, 835–844 (2003).

670   26.   Lindquist, B. E. & Shuttleworth, C. W. Adenosine receptor activation is responsible for

671   prolonged depression of synaptic transmission after spreading depolarization in brain

672   slices. *Neuroscience* **223**, 365–376 (2012).

673   27.   Bragin, A., Penttonen, M. & Buzsáki, G. Termination of epileptic afterdischarge in the

674   hippocampus. *J. Neurosci.* **17**, 2567–2579 (1997).

675   28.   Bonaccini Calia, A. *et al.* Full-bandwidth electrophysiology of seizures and epileptiform

676   activity enabled by flexible graphene microtransistor depth neural probes. *Nat.*

677   *Nanotechnol.* (2021). doi:10.1038/s41565-021-01041-9

678   29.   Bahari, F. *et al.* Seizure-associated spreading depression is a major feature of ictal

679   events in two animal models of chronic epilepsy. *bioRxiv* 455519 (2020).

680   doi:10.1101/455519

681   30.   Aquino-Cias, J., Belceva, S., Bureš, J. & Fifková, E. The influence of thalamic spreading

682   depression on cortical and reticular unit activity in the rat. *Brain Res.* **1**, 77–85 (1966).

683   31.   Fifková, E. Leao's Spreading Depression in the Thalamic Nuclei of Rat. *Experientia* **20**,

684   635–637 (1964).

685   32.   Dreier, J. P. The role of spreading depression, spreading depolarization and spreading

686   ischemia in neurological disease. *Nat. Med.* **17**, 439–447 (2011).

33.   Kramer, D. R., Fujii, T., Ohiorhenuan, I. & Liu, C. Y. Cortical spreading depolarization:

Pathophysiology, implications, and future directions. *J. Clin. Neurosci.* **24**, 22–27 (2016).

34. Kros, L., Lykke-Hartmann, K. & Khodakhah, K. Increased susceptibility to cortical

spreading depression and epileptiform activity in a mouse model for FHM2. *Sci. Rep.* **8**,

1–12 (2018).

35. Reiffurth, C., Alam, M., Zahedi-Khorasani, M., Major, S. & Dreier, J. P. Na+/K+-ATPase α

isoform deficiency results in distinct spreading depolarization phenotypes. *J. Cereb.*

Blood Flow Metab. **40**, 622–638 (2020).

36. Haglund, M. M. & Schwartzkroin, P. A. Role of Na-K pump potassium regulation and

IPSPs in seizures and spreading depression in immature rabbit hippocampal slices. *J.*

Neurophysiol. **63**, 225–239 (1990).

37. Takano, T. *et al.* Cortical spreading depression causes and coincides with tissue hypoxia.

Nat. Neurosci. **10**, 754–762 (2007).

38. Nicholson, C., Phillips, J. M., Tobias, C. & Kraig, R. P. Extracellular Potassium, Calcium

and Volume Profiles During Spreading Depression. in *Ion-Selective Microelectrodes and*

Their Use in Excitable Tissues (1981). doi:10.1007/978-1-4615-9224-2_22

39. Kraig, R. P., Ferreira Filho, C. R. & Nicholson, C. Alkaline and acid transients in

cerebellar microenvironment. *J. Neurophysiol.* (1983). doi:10.1152/jn.1983.49.3.831

40. Gorji, A. *et al.* Spreading depression in human neocortical slices. *Brain Res.* **906**, 74–83

(2001).

41. Chung, D. Y. *et al.* Determinants of optogenetic cortical spreading depolarizations. *Cereb.*

Cortex **29**, 1150–1161 (2019).

42. Houben, T. *et al.* Optogenetic induction of cortical spreading depression in anesthetized

and freely behaving mice. *J. Cereb. Blood Flow Metab.* **37**, 1641–1655 (2017).

43. Masvidal-Codina, E. *et al.* Characterization of optogenetically-induced cortical spreading

depression in awake mice using graphene micro-transistor arrays. *J. Neural Eng.* **18**,

(2021).

44. Sugimoto, K. *et al.* Peri-Infarct Hot-Zones Have Higher Susceptibility to Optogenetic

Functional Activation-Induced Spreading Depolarizations. *Stroke* **51**, 2526–2535 (2020).

45. Dell'Orco, M. *et al.* Repetitive spreading depolarization induces gene expression changes

related to synaptic plasticity and neuroprotective pathways. *Front. Cell. Neurosci.* **17**,

(2023).

46. Chever, O. *et al.* Initiation of migraine-related cortical spreading depolarization by

hyperactivity of GABAergic neurons and NaV1.1 channels. *J. Clin. Invest.* **131**, 1–15

(2021).

47. Zhou, N., Gordon, G. R. J., Feighan, D. & MacVicar, B. A. Transient swelling,

acidification, and mitochondrial depolarization occurs in neurons but not astrocytes during

spreading depression. *Cereb. Cortex* **20**, 2614–2624 (2010).

48. Shuttleworth, C. W. *et al.* Which Spreading Depolarizations Are Deleterious To Brain

Tissue? *Neurocrit. Care* **32**, 317–322 (2020).

49. Gorji, A. & Speckmann, E. J. Spreading depression enhances the spontaneous

epileptiform activity in human neocortical tissues. *Eur. J. Neurosci.* (2004).

doi:10.1111/j.0953-816X.2004.03436.x

50. Tamim, I. *et al.* Spreading depression as an innate antiseizure mechanism. *Nat.*

Commun. **12**, 1–15 (2021).

51. Heuser, K. *et al.* Ca 2+ Signals in Astrocytes Facilitate Spread of Epileptiform Activity.

Cereb. Cortex **28**, 4036–4048 (2018).

52. Enger, R. & Heuser, K. Astrocytes as critical players of the fine balance between

inhibition and excitation in the brain: spreading depolarization as a mechanism to curb

epileptic activity. *Front. Netw. Physiol.* **4**, 1–8 (2024).

53. Libbey, J. E. *et al.* Seizures following picornavirus infection. *Epilepsia* **49**, 1066–1074

(2008).

54. Enger, R. *et al.* Dynamics of ionic shifts in cortical spreading depression. *Cereb. Cortex*

25, 4469–4476 (2015).

55.   Wenzel, M., Hamm, J. P., Peterka, D. S. & Yuste, R. Reliable and Elastic Propagation of

Cortical Seizures In Vivo. *Cell Rep.* **19**, 2681–2693 (2017).

56.   Wenzel, M., Hamm, J. P., Peterka, D. S. & Yuste, R. Acute Focal Seizures Start As Local

Synchronizations of Neuronal Ensembles. *J. Neurosci.* **39**, 8562–8575 (2019).

57.   Truccolo, W. *et al.* Single-neuron dynamics in human focal epilepsy. *Nat Neurosci* **14**,

635–641 (2011).

58.   dal Maschio, M., Donovan, J. C., Helmbrecht, T. O. & Baier, H. Linking Neurons to

Network Function and Behavior by Two-Photon Holographic Optogenetics and

Volumetric Imaging. *Neuron* **94**, 774-789.e5 (2017).

59.   Andrasfalvy, B. K., Zemelman, B. V., Tang, J. & Vaziri, A. Two-photon single-cell

optogenetic control of neuronal activity by sculpted light. *Proc. Natl. Acad. Sci. U. S. A.*

107, 11981–11986 (2010).

60.   Couto, J. *et al.* Chronic, cortex-wide imaging of specific cell populations during behavior.

Nat. Protoc. **16**, 3241–3263 (2021).

61.   Peltola, M. E. *et al.* Routine and sleep EEG: Minimum recording standards of the

International Federation of Clinical Neurophysiology and the International League Against

Epilepsy. *Clin. Neurophysiol.* **147**, 108–120 (2023).

62.   Kager, H., Wadman, W. J. & Somjen, G. G. Conditions for the triggering of spreading

depression studied with computer simulations. *J. Neurophysiol.* **88**, 2700–2712 (2002).

63.   Weiss, S. A. *et al.* Ictal high frequency oscillations distinguish two types of seizure

territories in humans. *Brain* **136**, 3796–3808 (2013).

64.   Jung, R. Hirnelektrische Untersuchungen über den Elektrokrampf: Die Erregungsabläufe

in corticalen und subcorticalen Hirnregionen bei Katze und Hund. *Arch. F. Psychiatr. U.*

Z. Neur. **183**, 206–244 (1949).

65.   Andersen, P., Morris, R., Amaral, D., Bliss, T. & O'Keefe, J. *The Hippocampus Book*.

(Oxford University Press, 2006). doi:10.1093/acprof:oso/9780195100273.001.0001

66.   Henze, D. A., Wittner, L. & Buzsáki, G. Single granule cells reliably discharge targets in

the hippocampal CA3 network in vivo. *Nat. Neurosci.* **5**, 790–795 (2002).

67.   Scharfman, H. E. Hyperexcitability in combined entorhinal/hippocampal slices of adult rat

after exposure to brain-derived neurotrophic factor. *J. Neurophysiol.* **78**, 1082–1095

(1997).

68.   Shaw, K. *et al.* Neurovascular coupling and oxygenation are decreased in hippocampus

compared to neocortex because of microvascular differences. *Nat. Commun.* **12**, 1–16

(2021).

69.   Davolio, C. & Greenamyre, J. T. Selective vulnerability of the CA1 region of hippocampus

to the indirect excitotoxic effects of malonic acid. *Neurosci. Lett.* **192**, 29–32 (1995).

70.   Di Giacomo, R. *et al.* Stereo-EEG ictal/interictal patterns and underlying pathologies.

Seizure **72**, 54–60 (2019).

71.   Chevaleyre, V. & Siegelbaum, S. A. Strong CA2 pyramidal neuron synapses define a

powerful disynaptic cortico-hippocampal loop. *Neuron* **66**, 560–572 (2010).

72.   Whitebirch, A. C. *et al.* Enhanced excitability of the hippocampal CA2 region and its

contribution to seizure activity in a mouse model of temporal lobe epilepsy. *Neuron* **110**,

3121-3138.e8 (2022).

73.   Pernía-Andrade, A. J., Wenger, N., Esposito, M. S. & Tovote, P. Circuits for State-

Dependent Modulation of Locomotion. *Front. Hum. Neurosci.* **15**, 1–20 (2021).

74.   Arber, S. & Costa, R. M. Networking brainstem and basal ganglia circuits for movement.

Nat. Rev. Neurosci. **23**, 342–360 (2022).

75.   Fuhrmann, F. *et al.* Locomotion, Theta Oscillations, and the Speed-Correlated Firing of

Hippocampal Neurons Are Controlled by a Medial Septal Glutamatergic Circuit. *Neuron*

86, 1253–1264 (2015).

76.   Wirtshafter, H. S. & Wilson, M. A. Locomotor and Hippocampal Processing Converge in

the Lateral Septum. *Curr. Biol.* **29**, 3177-3192.e3 (2019).

77.   Mocellin, P. *et al.* A septal-ventral tegmental area circuit drives exploratory behavior.

Neuron **112**, 1020-1032.e7 (2024).

78.   Chung, J. E. *et al.* High-density single-unit human cortical recordings using the

Neuropixels probe. *Neuron* **110**, 2409-2421.e3 (2022).

79.   Paulk, A. C. *et al. Large-scale neural recordings with single neuron resolution using*

Neuropixels probes in human cortex. Nature Neuroscience **25**, (Springer US, 2022).

80.   Sellers, K. K. *et al.* Thin-film microfabrication and intraoperative testing of μeCoG and

iEEG depth arrays for sense and stimulation. *J. Neural Eng.* **18**, (2021).

81.   Lee, K. *et al.* Flexible, scalable, high channel count stereo-electrode for recording in the

human brain. *Nat. Commun.* **15**, (2024).

82.   Theodore, W. H., Porter, R. J. & Penry, J. K. Complex partial seizures: Clinical

characteristics and differential diagnosis. *Neurology* **33**, 1115–21 (1983).

83.   Bronsard, G. & Bartolomei, F. Rhythms, rhythmicity and aggression. *J. Physiol. Paris*

107, 327–334 (2013).

807