Branched and Linear F-actin Networks Control Directional Migration

Switching Behavior on Aligned Collagen Fibrils

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Abstract:

Directed cell migration is essential in biological processes like embryonic development, wound healing and cancer metastasis and is driven by a variety of directional cues, including aligned fibrils in the extracellular matrix (ECM), a phenomenon known as contact guidance. How different cells respond to aligned fibrils and how external factors like ECM stiffness and internal regulators like formins and Arp2/3 control contact guidance across different type of cells is unknown. In this study, a unique system to assemble aligned collagen fibrils on mica and to transfer them onto substrates with specified stiffness is used to probe how external factors and internal regulators affect contact guidance. This system reveals distinct contact guidance behaviors: mesenchymal cells exhibit high-fidelity contact guidance, amoeboid cells ignore cues and epithelial cells use a mixture of both parallel and perpendicular migration on aligned collagen fibrils. Formins and Arp2/3 exert reciprocal control over contact guidance across a variety of cell types, where formins mediators of linear F-actin structures enhance contact guidance and Arp2/3 a mediator of branched F-actin structures diminishes contact guidance. This controlled materials system reveals important external and internal mechanisms of how contact guidance directs cell migration across a variety of different cell types.

Graphical Abstract:

Abbreviations:

DPBS: Phosphate-Buffered Saline

BME (β-MercaptoEthanol)

APS: Ammonium Persulfate

APTES: 3-AminoPropylTriEthoxySilane

EGTA: Ethylene Glycol bis(2-aminoethyl ether)-N,N,N′,N′-Tetraacetic Acid

PVDF: Polyvinylidene DiFluoride

BSA: Bovine Serum Albumin

ECM: Extracellular Matrix

TEMED: N,N,N', N'-Tetraacetylethylenediamines

TBS: Tris Buffered Saline

HEPES: 2-hydroxyethylpiperazine-1-ethane sulfonic acid

FBS: Fetal Bovine Serum

DMSO: DiMethyl SulfOxide

MES: 2-N-Morpholino Ethane Sulfonic acid

ECL: Enhanced ChemiLuminescent

HFF: Human Foreskin Fibroblast

EMT: Epithelial to Mesenchymal Transition

AFM: Atomic Force Microscopy

p-myo: phosphorylated myosin

PAA: PolyAcrylAmide

af: Aligned Fibrils

tf: Transferred Fibrils

mdf: MultiDirectional Fibrils

rf: Random Fibrils

m: Mica

g: Glass

0.2: 200 Pa PAA gel

2: 2000 Pa PAA gel

20: 20,000 Pa PAA gel

1. Introduction:

Contact guidance refers to the directed migration of cells along aligned fibrils present in the extracellular matrix (ECM). Directional movement is crucial in a variety of biological processes. Studying contact guidance is particularly important because contact guidance controls embryonic development [1,2] and wound healing [3,4]. Contact guidance also impacts pathological conditions, directing migration in fibrosis and during cancer metastasis [5,6]. Contact guidance can be recreated *in vitro* using various methods, including electrospinning [7], which produces synthetic aligned fibrils; microcontact printing [8,9], which produces printed lines of ECM and grooves or ridges [10] that guide cellular movement topographically. While these are good at recapitulating certain geometric and chemical features, they lack ultrastructural signatures that are found on collagen fibrils assembled *in vivo*. Other approaches exist to make aligned collagen fibrils in 3D networks, including magnetic field alignment [11], mechanical rotation [12], flow-based alignment [13,14] or cell-based alignment [15–17]. Our lab has used a 2D self-assembly approach to make aligned collagen fibrils through epitaxial growth on mica, resulting in fibrils closely resembling those in tissues. We have developed methods to finely tune the structure of collagen fibrils on mica, allowing us to adsorb randomly oriented fibrils, bidirectional fibrils, aligned fibrils or no fibrils at all [18]. This approach allows for the observation of unique cellular responses to aligned collagen fibrils in comparison to other systems and has allowed for the characterization of the role of contractility and adhesion in tuning contact guidance, where mesenchymal cells contact guide well and amoeboid cells contact guide poorly [19]. These cell-type specific responses aren't visible with standard microprinting or topographical structures like ridges, but do replicate contact guidance behavior seen by mechanical alignment of collagen fibrils in 3D [12]. We also preliminarily explored a technique to transfer these fibrils onto glass, polydimethylsiloxane, and polyacrylamide gels [20], allowing us to initially probe how stiffness regulates contact guidance. Consequently, epitaxial growth of aligned collagen fibrils on mica affords a powerful approach to study contact guidance that retains ultrastructural characteristics of the collagen fibrils and mimics behavior seen in less tunable 3D contact guidance environments.

Cells within tissues have unique functions and, consequently, a unique set of genetic and signaling pathways that direct that behavior. The sensitivity of cells to contact guidance cues differs dramatically amongst cell types due to their differing roles within tissues. For instance, fibroblasts must remodel the ECM and generate contractile forces to provide mechanical stability of the wound. This frequently results in transient alignment of the ECM within the wound bed that enhances cell infiltration, including additional fibroblasts via contact guidance [3,21]. Over the long term, this alignment is destroyed once mechanical integrity and directed cell migration are no longer needed [22]. Epidermal keratinocytes on the other hand facilitate re-epithelialization outward in and may need to be less sensitive to fibril alignment, given that wounds frequently re-epithelialize uniformly from all directions [3]. Finally, immune

cells need to randomly surveil the wound microenvironment with no bias in migration in response to

aligned collagen fibrils, requiring them to ignore contact guidance cues. Indeed, ECM fibril alignment

seems not to enhance T cell infiltration into the tumor [23] and T cell contact guidance is low compared to

other cell types [24]. Local cell invasion during cancer occurs along aligned collagen fibrils that extend

radially from the tumor margin [25], but this primarily drives cancer cell and fibroblastic stromal contact

guidance. This suggests that cells can be placed into groups based on their roles and these groups of cells

have dramatically different abilities to sense and respond to contact guidance cues.

While early contact guidance work did not delineate between differences among cells of different

type, more recent work indicates that there are dramatic differences in how cells sense and respond to

contact guidance cues [26–29]. Different qualitative modes of migration have been described that have

allowed for a coarse-grain understanding of cell migration. Mesenchymal cells adopt a spindle shape,

showing strong adhesion and many stress fibrils, usually oriented parallel to the direction of migration.

Epithelial cells adopt a half-moon shape with a broad lamellipodium, intermediate adhesive strength, and

stress fibrils both parallel and perpendicular to the direction of migration. Amoeboid cells are rounded

with low adhesion and few stress fibrils but with a cortical contractile and protrusive F-actin cytoskeleton.

In addition, there are cells that can irreversibly or dynamically switch between epithelial and

mesenchymal migration modes as well as those that switch between amoeboid and mesenchymal modes

of migration [30,31]. Mesenchymal cells showed higher contact guidance than those undergoing epithelial-

to-mesenchymal transition (EMT) [28,32]. Ameboid cells showed random alignment, while mesenchymal

cells showed directed migration in both 2D and 3D systems [12,19]. However, these reports have mainly

been on substrates that may obscure cell type differences *in vivo* [19]. A systematic examination of contact

guidance across cell types in systems that present *in vivo* ECM structures is lacking. In particular, how

epithelial cells respond to contact guidance cues is not well understood. In addition, there is a lack of

understanding of how external signals like substrate stiffness and internal regulators of the F-actin

cytoskeletal control the cell type difference in contact guidance behavior.

Contact guidance occurs in tissues with a variety of different stiffnesses according to the needs of

the tissue. Stiffness can modulate a variety of different biophysical cellular aspects including traction

force and adhesion, two factors that regulate contact guidance. Consequently, it is reasonable that

stiffness affects contact guidance. Stiffness has been adjusted in various ways including increasing the

stiffness of individual fibers, tuning the underlying substrate stiffness and enhancing crosslinking of 3D

fiber networks [11,29,33–35]. On stiffer substrates, cells generate stronger traction forces, form more stable

adhesions, and align more effectively with the ECM fibrils, enhancing their directional migration along

these structures. In contrast, cells on soft substrates have weaker adhesions and traction forces, making

their alignment with ECM fibrils and directional movement less pronounced. Furthermore, there is some

indication that the most efficient contact guidance tends to be at physiological stiffness levels of the

substrate. While there are many disparate studies on contact guidance and how stiffness regulates it, there

is no systematic study on how stiffness regulates contact guidance across multiple cells.

Differences in contact guidance across different cells could be attributed to differences in surface

receptors, but in instances where cells spread and migrate on a particular substrate, likely differences in

contact guidance are due to signaling pathways and cytoskeletal regulation. The F-actin cytoskeleton is an

important regulator of cell migration. Cells build both linear and branched F-actin networks that allow the

cell to migrate directionally. Formins and Arp2/3 regulate cell migration by controlling the organization

of the actin cytoskeleton. Formins, promote the formation of linear actin filaments, which are essential for

creating stress fibrils and contractile forces that drive cell body movement and stabilize cell adhesion.

Arp2/3 on the other hand is responsible for forming branched actin networks, which are crucial for

generating the pushing forces needed for forming lamellipodia and protrusions at the leading edge of

migrating cells. There are only a few studies examining the role of Arp2/3 and formins in contact

guidance. Conflicting conclusions regarding the role of regulators like the Arp2/3 complex in managing

cell responses to contact guidance cues further complicate this landscape. While some studies suggest that

inhibiting Arp2/3 enhances cell alignment [36,37], others report the opposite [34]. What remains unknown is

the relationship between linear F-actin fibers and the enhanced contact guidance. Based on previous work,

it is likely that linear F-actin fibers are responsible for the stronger contact guidance, allowing cells to

better align and follow collagen fibrils. In contrast, branched F-actin fibers allow the cell to probe the

environment in many different directions and make turns and likely result in lower contact guidance.

In this paper, we use a fibril transfer technique to move native collagen fibrils assembled on mica

onto substrates with tunable stiffness. The contact guidance response of different cells with distinct

migration modes is explored in order to understand how cells with distinct cytoskeletal structures respond

differently to aligned collagen fibrils. We systematically assess how stiffness regulates contact guidance

and the role of myosin-mediated contraction in predicting contact guidance fidelity. We probe the balance

of linear and branched F-actin in determining contact guidance fidelity by assessing contact guidance

under both formins and Arp2/3 inhibition. Finally, we characterize a newly discovered epithelial

migration mode on aligned collagen fibrils. This mode of migration involves switching between parallel

and perpendicular migration with respect to aligned collagen fibrils. We explore the role of substrate

stiffness and the balance of formin-mediated linear F-actin and Arp2/3-mediated branched F-actin on

parallel and perpendicular migration of epithelial cells.

2. Materials and Methods:

2.1 Assembling collagen on mica

A freshly cleaved 15 mm x 15 mm piece of muscovite mica (highest grade VI, Ted Pella, Redding, CA) was used for the epitaxial growth of collagen fibrils. Rat tail collagen type I (Corning, Corning, New York) was diluted using 50 mM Tris-HCl (Fisher Scientific, Waltham, Massachusetts) and 200 mM KCl (Fisher Scientific, Waltham, Massachusetts) to achieve final concentrations of 10 or 100 μg ml^{-1} and added to the top of the mica. Following the 12-hour incubation period, the mica was washed with nano-pure water. The mica was then placed inside a tissue culture dish, allowed to dry overnight and used the following day. To prepare trimeric collagen structures on mica, 50 mM citric acid-sodium citrate (Fisher Scientific) and 200 mM KCl at pH 4.3 were used to dilute the collagen, and the mica was incubated as above.

2.2 Functionalizing and transferring collagen fibrils to glass

First, 22 mm × 22 mm coverslips (Corning, Corning, New York) were treated with piranha solution (3:1 H$_2$SO$_4$ (Fisher chemical) to H$_2$O$_2$ (Fisher chemical)) for 1 hour to ensure thorough cleaning and activation. After treatment, the coverslips were immersed in 1% (v/v) 3-aminopropyltriethoxysilane (APTES, Thermo scientific) solution prepared in 1 mM acetic acid (Alfa Aesarfor, Ward Hill, Massachusetts) for 2 hours to facilitate silanization. The coverslips were then thoroughly rinsed with deionized water and allowed to air dry. Subsequently, the coverslips were baked in an oven at 100 °C for 1 hour to promote covalent bonding of the APTES layer. Once cooled, the coverslips were treated with 6% (v/v) glutaraldehyde (Electron Microscope Science, Hatfield, Pennsylvania) in Dulbecco's Phosphate-Buffered Saline (DPBS) for 2 hours to introduce aldehyde functional groups. Following this treatment, the coverslips were extensively washed with deionized water to remove residual glutaraldehyde. Coverslips were good for two weeks. For transferring the collagen, 30% gelatin (Sigma Aldrich, St. Louis, Missouri) was dissolved in water and heated up to 40 °C for an hour, and 500 µl of the gelatin solution was placed on the mica with assembled collagen. After a 1-hour incubation, the gelatin was peeled off and placed on the target substrate, which was either chemically functionalized glass. Following an additional hour of incubation of the gelatin on the target substrate, the samples were washed with 5 ml of DPBS lacking magnesium and calcium (Gibco, Waltham, Massachusetts) by placing the DPBS inside the culture dish containing the substrate and incubating at 37 °C for 2 hours. After this period, the underside of the sample was cleaned with a Kim wipe (Kim wipe Kimberly-Clark, Irving, Texas), and the substrate was prepared for cell seeding.

2.3 Fabricating and transferring collagen fibrils to polyacrylamide gels

First, 22 x 22 mm coverslips were thoroughly cleaned and then covered with 0.1 M NaOH for 10 minutes.

Following this, the coverslips were treated with a 5% APTES solution for 5 minutes. The coverslips were

then washed three times with deionized water, each wash lasting 5 minutes. Next, a 0.5% glutaraldehyde

solution was applied to the coverslips for 30 minutes, followed by additional washes with deionized

water. To prepare polyacrylamide gels with different elastic moduli, solutions of 3%, 5%, and 8%

acrylamide and 0.03%, 0.1%, and 0.26% bis-acrylamide were prepared and 0.05% Ammonium Persulfate

(APS, Bio-Rad, Hercules, California) and 0.15% N,N,N', N'-Tetramethylethylenediamine (TEMED,

Fisher Scientific), respectively, to achieve gels with elastic moduli of 200, 2000, and 20000 Pa [38].The

functionalized coverslips were placed face down onto drops of these solutions on microscope slides,

allowing polymerization to occur for 20 minutes. The samples were then treated with 2 mM Sulfo-

SANPAH (Thermo Scientific) under UV light for 8 minutes to functionalize their surfaces. For the

subsequent steps, either the fibril transfer technique was employed as described above for glass or, in the

case of preparing trimer samples, the coverslips were exposed to 100 μg ml^{-1} collagen dissolved in 0.01 M

acetic acid overnight in the fridge.

2.4 Characterizing collagen fibrils using Atomic Force Microscope (AFM) imaging and

immunofluorescence

The topography of the collagen assembly on mica and transferred to glass was imaged using an AFM

(Digital Instruments, now Bruker Nano, Santa Barbara, CA) multi-mode AFM in tapping-mode with

TESPA probes with 40 mV drive amplitude and frequency of 320 kHz. Captured images were processed

with the plain fit and flattened routines as appropriate. Collagen fibrils were also stained and imaged

using immunofluorescence. Collagen fibril samples were first blocked with blocking buffer (0.02 g ml^{-1}

BSA prepared in 10% TBS containing 0.01% Tween-20) for 20 minutes and then incubated with 1:100

collagen antibody (polyclonal rabbit, Thermo fisher, Bio-Rad-2150-1908) for 24 hours. After washing

three times with 1x TBS for 5 minutes each, samples were incubated with a 1:200 dilution of donkey anti-

rabbit 488 (Jackson Immuno Research, #711-035-152) secondary antibody for 1 h, followed by additional

washes.

2.5 Culturing cells and treating with inhibitors

An immortalized human foreskin fibroblast cell line (HFF, ATCC, Manassas, VA), a human mammary

carcinoma cell line (MDA-MB-231, ATCC), a metastatic human melanoma cell line (WM-266-4,

ATCC), an immortalized human keratinocyte cell line (HaCaT, kind gift from Dr. Torsten Wittmann) and

an immortalized monocyte cell line (THP-1, ATCC) were used. MDA-MB-231s, WM-266-4 and HaCaTs

were cultured in Dulbecco's modified Eagles medium (DMEM, Sigma Aldrich). It was supplemented

with 10% fetal bovine serum (FBS) (Gibco, Grand Island, New York, USA), 1% penicillin–streptomycin

(Gibco), and 1% Glutamax (Gibco) at 37 °C in 5% CO_2. The same media with 15% FBS (Gibco) was

used for culturing HFF cells. THP-1 cells were cultured in RPMI-1640 media with 10% FBS, 1%

Penstrep, 0.05 mM BME (β-Mercaptoethanol). When live cells were imaged, cells were placed in culture

media Dulbecco's Modified Eagle Medium that lacked phenol red, but contained 15 mM 4-2-

hydroxyethyl) piperazine-1-ethanesulfonic acid (HEPES), 1x Glutamax, 1x penicillin/streptomycin, 10%

Fetal bovine serum (FBS). For inhibitor treatments, cells were centrifuged, counted and suspended in

culture media. SMIFH2 (Millipore), CK-666 (Millipore) and blebbistatin (Millipore) were dissolved at 50

mM, 50 mM and 20 mM stock solutions in dimethyl sulfoxide (DMSO). Stock solutions of the inhibitor

were diluted in either culture media or imaging media by at least 1000-fold to make working solutions of

0.5, 5, 10, 20, and 50 mM. For the control group, 0.1% DMSO was added to cell culture media or imaging

media.

2.6 Immunofluorescence imaging and analyses

Cells were plated onto target substrates at concentration of 20,000 cells ml^{-1} for subsequent experiments.

Cells were fixed and stained to visualize their F-actin structure and quantify their response to contact

guidance through morphology and alignment behavior. First, the cells were treated with 4%

paraformaldehyde (Fisher Scientific) for 10 minutes, prepared by diluting 16% paraformaldehyde in a

cytoskeleton buffer consisting of 10 mM 2-N-morpholino ethane sulfonic acid (MES, pH 6.1, Fisher

Scientific), 3 mM $MgCl_2$ (Fisher Scientific), 138 mM KCl (Fisher Scientific), and 2 mM EGTA (Sigma

Aldrich). Next, cells were permeabilized using a 0.5% Triton-X (Fisher Bioreagents) solution in the

cytoskeletal buffer for 5 minutes. Unreacted aldehydes were then blocked with 100 mM glycine (Fisher

Scientific) for 15 minutes. Cells were washed three times with 1x Tris Buffered Saline (TBS) for 5

minutes each. Cells were stained with Alexa 488-phalloidin (Thermo Fisher Scientific) for 1 hour and

DAPI (Sigma) for 15-30 minutes in 1x TBS containing 0.1% (v/v) Tween-20 (Fisher Bioreagent) and 2%

(w/v) Bovine Serum Albumin (BSA, Sigma Life Science). For phospho-myosin and anti-paxillin staining,

after initial phalloidin staining and washing with 1x TBS, cells were incubated with 1:50 dilution of

phospho-myosin antibody (Cell Signaling, mouse, 3675) or a 1:200 dilution of anti-paxillin primary

antibody (BD Biosciences, mouse, 610051) for 24 hours at 4 °C. Samples were then washed with 1x TBS,

followed by incubation with a 1:200 dilution of donkey anti-mouse IgG secondary antibody (Jackson

ImmunoResearch, 715-175-150) and 1:500 dilution of DAPI for 1 hour. Samples were washed again with

1x TBS three times for 5 minutes each. To improve image resolution, Prolong Gold mounting media

(Thermo Fisher) was applied between the substrate with cells and the cover slides. Samples were sealed

with VALAP (a mixture of Vaseline, lanolin, and paraffin) and imaged the next day using epifluorescence

microscopy with 10x, 40x, and 60x objectives ($NA = 0.3$, $NA = 1.3$, and $NA = 1.49$, Nikon). The

immunofluorescence images were analyzed with ImageJ. Lines around the cell's edge were drawn and an

oval was fit to the cell shape. The aspect ratio was calculated as the ratio of the major axis of the cell

divided by the minor axis of the cell. The angle of the cell was calculated as the angle between the long

axis of the cells and the horizontal vector of the image. To quantify the directionality of fixed cells, the

migration vector was analyzed using Python. The Directionality Index (DI) was calculated as the

$\cos(2|\Delta\theta|)$, where $|\Delta\theta|$ represents the angular deviation of the cell from the average cell angle in the

region. Cells with an area less than 300 μm^2 and an aspect ratio less than 1.5 were assigned a random

number for their angle to calculate the average angle of the region as their specific direction was not

readily calculatable. Then we used that angle to calculate a DI for all cells. If the area was less than 300

μm^2 then the DI was not included in the calculation. However, for THP-1 cells, which are small and do

not spread, applying a threshold of 300 μm^2 results in the exclusion of almost all data. Therefore, we

included all data points in the calculation of the DI for THP-1 cells. For the calculation of area and aspect

ratio, all cells were included.

2.7 Western blotting

We employed Western blotting to quantify phosphorylated myosin expression across different cell lines.

Using two million cells from different mammalian cell lines (HFF, HaCaT, MDA-MB-231, WM-266-4,

and THP-1 cells) at an approximate confluency of 80% in a cell culture dish, cells are washed with 1x

PBS and trypsinized, counted and centrifuged in a conical tube to form a pellet. A total of 100 μl of 1x

sample buffer was added to the tube. The cells in the tube were lysed on ice with a conical pestle to

ensure cells formed a uniform lysate. Protein lysate was heated at 94 °C for 5 minutes. Proteins were

separated on 4-20% precast polyacrylamide gel (Bio-Rad, Min-PROTEAN® TGX Stain-Free™ Protein

Gels, 10 well, 30 μl, 4568093) by loading a total of approximately 90 μg of protein lysate for each cell

line in the gel wells, running the gel at 120 V for 1 hour and transferring it onto a polyvinylidene

difluoride (PVDF) transfer membrane (Thermo-Fisher Scientific, PB9220) at 100 V for 1 hour and 30

minutes. The blot was blocked in PBST, and 5% skim dried nonfat milk at 37 °C for 1 hour. The

membrane was incubated in primary phospho-myosin antibody (Cell Signaling, mouse, 3675, 1:200

dilution) and or β-actin antibody (Santa Cruz, mouse, C-2, sc-8432, 1:500 dilution). Antibodies were

incubated at 4 °C overnight, washed using washing buffer three times for 5 minutes, followed by

treatment with donkey anti-mouse secondary antibody (Jackson ImmunoResearch, 715-035-150, 1:500)

incubated for 1 hour, then the membrane was rewashed three times for 5 minutes. Blots were developed

using freshly prepared enhanced chemiluminescent (ECL) reagents (250 mM luminol in DMSO, 90 mM p-

coumaric in DMSO acid,1 M Tris-HCI pH 8.5, 30% H_2O_2 and water) and visualized using Bio-Rad Gel

Doc XR+ Imaging system. Lastly, to quantify the protein bands, we used Image J software. Band

intensities on the immunoblot were quantified by selecting a rectangular region of interest around the

band as well as one around a background region locally. The intensity of the background region was

subtracted from the intensity of the band region. This value was divided by the corresponding background

subtracted value for β-actin as a loading control.

2.8 Quantifying gel compaction

For the gel compaction experiment, cells were embedded in a 2 mg ml^{-1} or 1.5 mg ml^{-1} collagen gel,

where the optimum percentage of DMEM and FBS were maintained depending on specific cell lines. To

achieve that, a solution of 5x DMEM, 10x FBS, and 10^7 cells ml^{-1} mixture was used to achieve a final

percentage of 1x DMEM, 10 or 15% FBS, and concentration of cells corresponding to each cell line

mentioned above. To neutralize the acidic collagen gel compaction mixture, 0.1 M filter sterile NaOH was

employed. Finally, filter-sterilized deionized water was used to attain a total volume of 500 µl collagen

gel compaction mixture. After thoroughly mixing the collagen gel compaction mixture by avoiding air

bubble formation, the mixture was put into a pre-sterilized cylinder shaper placed in a 6-well dish. Then

the gel was incubated for 2 hours at 37 °C for gel formation, the cylinder shaper was removed and 2 ml of

corresponding cell culture media was added to the gel to produce a floating gel in media. Gel images were

taken at 0, 4, 20, 32, 54, 72, 96, 132, and 140 hours to observe the change in gel diameter. For the

SMIFH2 and CK-666 inhibitor-treated gel compaction experiments, final concentrations of 20 and 50 µM

SMIFH2 and 5 and 25 µM CK-666 were achieved within both collagen gel and media around the gel to

avoid concentration differences due to diffusion. Obtained images were analyzed in ImageJ to measure

the gel diameter at different times corresponding to the degree of compaction. The gel diameter at

different time points was analyzed using GraphPad Prism 8, where non-linear regression analysis for a

two-phase decay model was performed. To determine the fractional compaction, the gel diameter at 48

hours for each replicate was calculated using the two-phase decay equation. The fractional compaction is

then defined as the ratio of the change in diameter from 0 hours to 48 hours, relative to the diameter at 0

hours.

2.9 Live cell migration imaging and analyses

Chambers were fabricated by cutting adhesive heat resistant thin transparent silicone rubber sheets using a

craft cutter to form a chamber on a glass surface. This chamber is filled with clear media, supplemented

with 10-15% FBS, depending on the cell line. Once the media is prepared, the substrate with the cells is

flipped over onto the chamber. The chamber is sealed with VALAP. The setup is then imaged over an 8-

hour period with images captured at 2-minute intervals. This allows for detailed observation and analysis

of cell migration behavior. The DI calculations for live cell migration were based on the average of

$\cos(2|\Delta\theta|)$, with $|\Delta\theta|$ being the angle difference between the fibrils and the cell's direction, derived from

changes in x and y positions at 2-minutes intervals and averaged over 8 hours. Speed was calculated by

averaging the displacements measured every 2 minutes, dividing the total displacement over the 2

minutes by the corresponding time interval, and then averaging the resulting speeds over 8 hours. To

categorize migration direction during live cell migration, the direction of cell movement was calculated

over a 12 minute window every six 6 minutes. The number of steps was classified based on deviation

angles: less than 30°, between 30° and 60°, and greater than 60°, using R for analysis. Steps with speeds

less than 10 μm/hour were considered slow.

2.10 Assessing statistical significance

Statistical significance was assessed using a 95% confidence interval, calculated from the experimental data

and placed on graphs in the form of error bars. Nonoverlapping confidence intervals indicate statistical

significance to approximately $p < 0.05$.

3. Results:

3.1 Self-assembled collagen fibrils transferred to glass induce robust fibroblast alignment

Collagen fibrils can be epitaxially assembled on mica via electrostatic interactions between the collagen fibrils and the mica. Under specific buffer conditions which include collagen concentration and adsorption time, well-aligned collagen fibrils can be formed and imaged using AFM. Ultrastructural characteristics like D-banding as observed *in vivo* are formed (**Figure 1A**). We have previously shown collagen fibril alignment across large swaths of the substrate [18]. Similar collagen fibril structure can be seen on the transferred substrates as imaged by immunofluorescence (**Supplementary Figure 1**). While the collagen intensity after transfer was higher than that on mica, this is likely due to residual gelatin left after transfer that can be recognized by the collagen antibody. Collagen level is similar on all transferred substrates indicating similar transfer efficiency (**Supplementary Figure 1**). Human foreskin fibroblasts (HFFs) readily align and migrate along the collagen fibrils (**Figure 1A&B**). However, because of their contractile nature, they pull the collagen fibrils from the mica substrate after about 1 hour, culminating in complete collagen fibril delamination at around 4 hours (**Figure 1A&B**). This catastrophic delamination timing is cell density-dependent, occurring at different times across the substrate, leading to high variability in the fraction of cells that remain at 4 h (**Figure 1B**). We assessed whether delamination occurred on other substrates. We adsorbed collagen trimers (t) to mica using low pH, assembled aligned collagen fibrils (af) on mica, created multi-directional collagen fibrils (mdf) by using higher collagen concentrations and transferred aligned collagen fibrils (tf) to functionalized glass. AFM images verified that the solution conditions and transfer approach created the desired fibril morphologies (**Figure 1C**). Cell alignment was quantified using a directionality index. The directionality index was calculated by finding the deviation of the individual cell alignment direction with respect to the average cell alignment direction within one image and using this angle in the directionality index calculation as outlined in the materials and methods. Directionality index values of 1 indicate high alignment with collagen and high-fidelity contact guidance and values of 0 indicate low alignment with collagen and low contact guidance fidelity. HFFs were not well spread or aligned on trimers (**Figure 1D**). On aligned collagen fibrils assembled on mica, cells were aligned well initially (1 hour), but eventually detached due to collagen delamination (4 hours), leaving both large clusters as well as a small number of single cells that were not well aligned (**Figure 1E**). Multi-directional collagen fibrils induced better spreading than the trimers, but the cell appeared confused and directional alignment was poor. Transferred collagen fibrils resulted in robust spreading and alignment of HFFs due to the chemical linkage of the collagen fibrils to the glass surface. Consequently, HFFs, mesenchymal cells that are known to be highly contractile cells engage in robust contact guidance on aligned collagen fibrils, but not on other non-aligned collagen substrates. Furthermore, collagen delamination and deadhesion of cells only occurs on aligned collagen fibrils

assembled on mica. Consequently, long-term HFF alignment is only observed on collagen fibrils

transferred to glass (**Figure 1E**).

3.2 Optimal contact guidance occurs at different stiffnesses depending on the cell type

Given that HFFs robustly spread and orient on aligned collagen fibrils, but only when collagen fibril

delamination was blocked by transferring collagen fibrils to glass, we examined whether this behavior

was observed in other cell lines. Previously, we showed that carcinoma cells that adopt a mesenchymal

mode of migration (MDA-MB-231) tended to robustly orient and directionally migrate on aligned

collagen fibrils, whereas carcinoma cells that adopt an amoeboid mode of migration (MTLn3) did not

[18,19]. Along with HFF and MDA-MB-231 cells, we examined WM-266-4, HaCaT, and THP-1 cells.

WM-266-4 cells are a mesenchymal to amoeboid mode-switching cell line.[31] HaCaTs migrate as

epithelial cells. THP-1 cells are a model naive immune cell that moves with an amoeboid migration mode.

We examined the orientation of individual cells across different cell lines on collagen fibrils assembled on

mica as well as those transferred to glass (**Figure 2A**). The delamination of collagen fibrils assembled on

mica was observed in response to HFF (**Figure 1**) or MDA-MB-231 [20] cells that is blocked when

collagen fibrils are transferred to glass. This suggests that the perceived stiffness that the cell experiences

is lower on fibrils adsorbed to mica compared to those transferred to glass and that this might control the

cell response to aligned collagen fibrils. HFF and MDA-MB-231 cells adopted extended, large area

morphologies with long stress fibers in the direction of the long axis of the cell, typical of mesenchymal

cells. However, HFF cells had a wider body and more pronounced F-actin stress fibrils within and

paxillin focal adhesions underneath the cell body (**Figure 2B**). WM-266-4 and HaCaT cells adopted an

epithelial cell morphology with numerous different types of F-actin fibrils including longitudinal stress

fibers and transverse arcs that terminated in large focal adhesions (**Figure 2B**). Finally, THP-1 cells were

not well spread, did not include well-defined F-actin fibers and only had small focal adhesions (**Figure**

2B). HFF cells spread to the greatest extent and adopted spread areas roughly 4-fold larger than any of the

other cell lines. Interestingly, the spread area did not differ dramatically between aligned collagen fibrils

assembled on mica and those transferred to glass except for HFFs and HaCaTs, where areas for both cell

lines were larger when the collagen fibrils were transferred to the stiff glass substrate (**Figure 2C**). The

degree of directional alignment differed dramatically across the cell lines. HFF and MDA-MB-231 cells

robustly oriented on aligned collagen fibrils, whether the collagen fibrils were assembled on mica or

transferred to glass (**Figure 2D**). WM-266-4 cells oriented well on aligned collagen fibrils assembled on

mica, but poorly on those transferred to glass. HaCaTs adopted an intermediate degree of orientation,

whereas THP-1 cells adopted a poor degree of orientation on aligned collagen fibrils. Both HaCaTs and

THP-1s did not show differences across the two substrates. The trends in aspect ratio were similar to

those in directionality index, indicating that aspect ratio is a reasonable proxy for contact guidance ability

(**Supplementary Figure 2**). Consequently, mesenchymal cells were best at orienting on aligned collagen

fibrils, followed by cells that adopt an epithelial morphology. Amoeboid cells were worst at orienting on

aligned collagen fibrils. Furthermore, there are substrate-specific differences in responses to aligned

collagen. HFFs and HaCaTs were better spread on the stiff substrate (glass), whereas MDA-MB-231 and

WM-266-4 cells were better aligned on the soft substrate (mica).

Given that some cell lines directionally migrate better on collagen fibrils chemically attached to

stiff glass substrates, while others prefer collagen fibrils that are loosely attached to mica, we explored the

role of both external mechanical properties of the substrate and internal contractile force generation

properties of the cell lines. Many of the cell lines showed measurable, but modest dependence of

directionality on stiffness, except for WM-266-4 cells, which showed a large and steadily declining

directionality for increasing stiffness (**Figure 3A**). We observed a different stiffness for maximal

directional alignment across the cell lines. HFFs appeared to align best on 0.2 kPa, MDA-MB-231 and

WM-266-4 cells aligned best on mica and HaCaTs aligned best on 2 kPa. The poor directionality of THP-

1 cells hindered determining the stiffness of optimal directional migration. Areas and aspect ratios were

roughly the same for the cells across stiffnesses, except for HFFs and HaCaTs, which showed robust

increases in area as stiffness increased (**Supplementary Figure 3A-C**). Studies have indicated a

correlation between directionality and internal cell contractile force, which is associated with myosin

activity, a motor protein in cells [8,12,19,39,40]. We hypothesized that cells with higher directionality would

exhibit higher levels of phosphorylated myosin (p-Myo). Initially, we considered fibril patterns that test

this hypothesis and measured phosphorylated myosin immunofluorescence. Interestingly, cells with

roughly similar shapes showed variability in phosphorylated myosin level (**Figure 3B**). Also, conditions

that produced the highest directionality had the lowest phosphorylation level (mica) (**Figure 3C**). This

differed somewhat from cells on a non-directional collagen cue (collagen trimers on glass), where there

appeared to be an increase in phosphorylated myosin as has been seen previously. Cells plated on

collagen trimers attached to 0.2 kPa PAA (Polyacrylamide) gel were essentially unspread and showed

extremely high signal. However, it is important to note that high phosphorylated myosin level is only

efficacious if coincident with a contractile F-actin structure and adhesion to the substrate. Challenges in

accurate quantification of immunofluorescence images led to our assessing myosin phosphorylation and

contraction by two different means: western blotting and collagen gel compaction. Interestingly, the

maximal directionality for each cell type correlated well with the phosphorylated myosin level as

measured by western blot (**Figure 3D and Supplementary Figure 3E**). To further assess contractility,

we conducted a compaction test. Cells compact collagen gels at different rates (**Supplementary Figure**

3D). The fractional compaction can be defined as the ratio of gel diameter change relative to the initial

diameter over 48 hours. The results showed that HFF and MDA-MB-231 cells, both exhibiting

mesenchymal migration with the highest directionality, had the highest fractional compaction (**Figure**

3E). HaCaTs showed lower compaction, followed and WM-266-4 and THP-1 which did not compact

gels. Consequently, the directionality of cells was both stiffness and cell type dependent. In addition,

contact guidance ability correlated strongly with both phosphorylated myosin as measured by western

blot and fractional compaction, two measures of the ability of cells to generate and transmit contractile

force.

3.3 Formins regulate cell migration parallel to aligned collagen fibrils, while Arp2/3 controls

movement perpendicular to collagen fibrils

In order to explore why different cells on different substrates engage in contact guidance to different

extents, we perturbed the F-actin cytoskeleton. Different cells use unique F-actin regulatory machinery to

form a particular cell shape and migrate with a particular mode. Two important classes of F-actin

regulatory proteins are Arp2/3 and the formins family of F-actin regulators. Arp2/3 forms branched F-

actin, whereas formins regulate the formation of linear F-actin. Broad lamellipodia formed by branched F-

actin networks likely give the cell the ability to make turns during migration, whereas aligned stress

fibrils have been found to be important in contact guidance [19]. In addition, branched F-actin and linear F-

actin draw G-actin from the same pool, creating a tempting hypothesis that when one type of network is

diminished, the cell can build the other type of network [41]. Consequently, we hypothesized that these F-

actin regulators control contact guidance in distinct ways. To test this hypothesis, we employed

pharmacological agents including SMIFH2, a formin inhibitor, and CK-666, an Arp2/3 inhibitor.

Inhibition of formins with SMIFH2 in HFF and MDA-MB-231 cells, resulted in dramatic

morphology changes (**Figure 4A**). Cells were smaller (**Supplementary Figure 4A&B**) and had

diminished stress fiber formation and smooth edges suggestive of branched F-actin networks. Similar

morphological responses were seen on both aligned collagen fibrils on mica and aligned collagen fibrils

transferred to glass. In addition, cells treated with SMIFH2 showed marked decrease in directionality

(**Figure 4B&C**) and aspect ratio (**Supplementary Figure 4C&D**) at high concentrations. The decrease in

directionality of cells plated on aligned collagen fibrils transferred to glass is small, but measurable at 20

μM, increasing through 50 μM, whereas cells plated on aligned collagen fibrils assembled on mica seems

to require higher SMIFH2 concentrations to achieve measurable changes in directionality. Given the

correlation observed between directionality and contractility and that SMIFH2 is known to block myosin

activity at high concentrations (> 50 μM) [42], we measured contractility in two different ways. First, we

plated cells on collagen fibrils assembled on mica with and without 20 μM SMIFH2 and measured the

kinetics of fibril delamination (**Figure 4D**). There was a small increase in fraction of cells remaining, but

it was not statistically significant. This suggests that contractility at this concentration was not

dramatically inhibited. Compaction kinetics showed a different response (**Supplementary Figure 4E**).

Both 20 and 50 μM diminished compaction as compared to untreated cells (**Figure 4E**). Consequently,

inhibiting formins diminishes stress fibril formation and modestly diminishes directionality at

concentrations that likely do not affect myosin activity. At higher formins inhibitor concentrations,

myosin is likely inhibited, resulting in dramatic alterations in directionality as we have demonstrated

previously [43]. Interestingly, formin inhibition more robustly affects compaction, even at low

concentrations. This indicates that formin-mediated F-actin cytoskeletal structures contributes to contact

guidance.

Given that linear F-actin fibrils facilitated by formin activity enhance directionality during contact

guidance, we were interested in assessing the role of Arp2/3-mediated branched F-actin networks in

contact guidance. Inhibition of Arp2/3 with CK-666 in HFFs resulted in very few morphological changes

(**Figure 5A**). However, treatment with CK-666 resulted in increased directionality compared to control

cells, indicating that Arp2/3 activation inhibits contact guidance (**Figure 5B**). We assessed whether

Arp2/3 inhibition could affect the cells ability to delaminate collagen fibrils. It did not, suggesting myosin

activity was not greatly altered (**Figure 5C**). Additionally, inhibiting Arp2/3 showed only a small

decrease in gel compaction (**Figure 5D** and **Supplementary Figure 5**). Even if Arp2/3 inhibition were to

affect compaction through diminishing myosin contractility, the known effect on contact guidance in

response to diminished myosin contraction would have been to diminish contact guidance. However, this

was not the case as there was a measurable increase in directionality under Arp2/3 inhibition.

Consequently, Arp2/3 likely acts to inhibit contact guidance through the production of branched F-actin

networks that give cells an ability to change directions by partially ignoring contact guidance cues. Taken

together with data above, formins enhances contact guidance whereas Arp2/3 diminishes contact

guidance.

3.4 The switch-like directional migration behavior of HaCaT cells can be modulated by

manipulating both formins and Arp2/3

We have previously established that mesenchymal cells robustly engage in contact guidance on aligned

collagen fibrils. Epithelial cells on the other hand seem to be less robust in their alignment (**Figure 2 &**

3). Consequently, they may be a better model system by which to assess whether formins or Arp2/3

inhibition can increase or decrease cell alignment. However, it is difficult to determine the direction of

HaCaT cell migration in fixed images, due to the fact that they are less aligned than mesenchymal cells.

Consequently, we examined HaCaT migration on aligned collagen fibrils assembled on mica (low

stiffness) or transferred to 2 kPa PAA gel (moderate stiffness) or glass (high stiffness). Montages of live

cell migration showing images at 0, 2, 4, and 8 hours on these substrates revealed interesting behavior

(**Figure 6A**). Unlike mesenchymal cells which migrate solely parallel to collagen fibril alignment [18,19],

HaCaT cells migrated both parallel to the collagen fibrils as well as perpendicular to collagen fibrils,

exhibiting a switching behavior (**Figure 6A**). Both parallel and perpendicular movement additionally

complicates interpretation of contact guidance from fixed cells. Consequently, we assessed migration

directionality on these different substrates. Indeed, directionality was lower on both collagen fibrils

assembled on mica and those transferred to 2 kPa PAA when measured by migration as compared to

morphology (**Figure 6B**). Directionality index increased with substrate stiffness, progressing from mica

to glass (**Figure 6B**). Interestingly, cell speed exhibited an inverse trend (**Figure 6C**), demonstrating that

stiffer substrates slow down cell migration but enhance its directedness. In order to understand the reason

for changes in directionality, given migration both parallel and perpendicular to collagen alignment, we

measured the residence time that a cell remains in either in parallel (migration angle < 30° with respect to

the aligned fibril direction) or perpendicular (migration angle > 60° with respect to the aligned fibril

direction) movement. While HaCaT cells spend more time migrating parallel to the collagen fibrils, they

do spend a considerable amount of time migrating perpendicularly (**Figure 6D**). HaCaT cells spend more

time in parallel movement on stiffer substrates (collagen fibrils transferred to glass) than on softer

substrates (collagen fibrils assembled on mica). This agrees with the data showing that HaCaT cells

migrating on collagen fibrils transferred to glass have a higher directionality index. In addition to

residence time, we quantified the fraction of the time cells migrate in a parallel or perpendicular manner

with respect to the fibrils with a more stringent criterion. Migration parallel to fibril direction was defined

as a migration angle < 30° with respect to the aligned fibril direction, whereas migration perpendicular to

fibril direction was defined as a migration angle > 60° with respect to the aligned fibril direction (**Figure

6E**). Increased stiffness diminished perpendicular movement compared to parallel movement, but

migration on the 2 kPa PAA substrate showed the most evenly balanced parallel and perpendicular

movement. Consequently, unlike mesenchymal cells, epithelial cells have two modes of directed

migration on aligned collagen fibrils, one that is parallel and one that is perpendicular. Furthermore, the

stiffness of the underlying substrate can tune the dominance of one of these modes of migration over the

other.

Given that HaCaT cells have intermediate directionality and that they have both parallel and

perpendicular movement, we were interested in assessing the role of formins and Arp2/3 in controlling

directionality and the balance of these different directional migration modes. As demonstrated in the

previous section, formins enhance directionality, whereas Arp2/3 diminishes directionality. A hypothesis

that flows from this observation is that formins enhance parallel movement, whereas Arp2/3 enhances

perpendicular movement. We fixed HaCaTs plated on aligned collagen fibrils transferred to glass after

formins or Arp2/3 inhibition (**Figure 7A**). Inhibiting formins results in larger cells that seem to be

directionally confused, whereas inhibiting Arp2/3 results in a similar morphology as compared to control

with only modest directional confusion. To complement fixed cell morphology, HaCaTs were imaged

during migration. Montages are shown containing images at 0, 2, 4, and 8 hours (**Figure 7B**). As

described in Figure 7A, formin inhibition appears to enhance cell area and both formin and Arp2/3

inhibition seem to increase directional confusion and cell migration speed (**Figure 7B**). We quantified

directionality index and speed. Directionality index assessed by fixed cells and in live cells decreased

robustly when formins were inhibited as we described above (**Figure 7C**). Inhibition of Arp2/3 only

modestly reduced directionality (**Figure 7C**). Speed showed a different response. Cells under formin or

Arp2/3 inhibition moved at the same rate as each other as well as faster than controls (**Figure 7D**). Since

HaCaT cells move in both parallel and perpendicular fashions, we assessed whether inhibiting formins or

Arp2/3 differentially affected these different directional modes of migration. Similar to our previous

analyses (**Figure 6**), we quantified and analyzed cell movements to evaluate the effects of formins or

Arp2/3 inhibitors. Decreases in residence time (**Figure 7E**) tracked with changes in directionality index

(**Figure 7C**). For cells treated with the Arp2/3 inhibitor (25 µM CK-666), we observed an increase in both

parallel and perpendicular steps (**Figure7F**), resulting in a slightly lower directionality index, compared

to the control due to the balanced distribution between parallel and perpendicular movements (**Figure

7C**). In contrast, cells treated with the formin inhibitor (20 µM SMIFH2) showed a similar fraction of

parallel steps compared to the control but an increased fraction of perpendicular movements, resulting in a

markedly lower directionality than the control. These results for epithelial cells agree with the above

results for mesenchymal cells. Formins tend to enhance parallel migration of epithelial cells, whereas

Arp2/3 has more subtle effects, including diminishing the fraction of parallel moving cells.

To further establish that the formin inhibitor was not simply blocking myosin activity indirectly

to alter contact guidance, we investigated the role of myosin contractility in contact guidance by

perturbing contractility using blebbistatin (bleb). Blocking myosin diminished directionality and

increased cell speed (**Supplementary Figure 7B&C**), consequences that we have described in

mesenchymal cells elsewhere [19]. Interestingly, when assessing various concentrations of SMIFH2, a

notable trend emerged. At 10 µM SMIFH2, the directionality index exhibited a significant increase,

approaching control levels (**Supplementary Figure 8**). This behavior was also observed in live cell

migration analyses (**Figure 8**), where the directionality index for 10 µM SMIFH2 was closer to the control

than the 20 µM SMIFH2 condition. To explore whether diminished myosin activity explained the decrease

in directionality index and increase in speed moving from 10 µM SMIFH2 to 20 µM SMIFH2, we treated

cells with both 10 µM SMIFH2 and 3 µM blebbistatin. This did not diminish directionality index to the

same extent as either 3 µM blebbistatin or 20 µM SMIFH2 alone. This indicates that the formin inhibitor is

uniquely affecting contact guidance and does not simply act as a myosin inhibitor. All inhibitor

conditions for HaCaTs were then plotted on the same speed and directionality index graph. Interestingly,

a biphasic response is seen, whereby speed increases dramatically, when directionality index is somewhat

diminished, but when directionality index highly diminished speed decreases (**Figure 8**). This indicates

that there is a coupling between how fast cells move and how directional they are and these parameters

are not independently controlled through the myosin/formin/Arp2/3 pathways. In summary, our findings

highlight the significant roles of formins and Arp2/3 in regulating contact guidance that are distinct from

myosin.

4. Discussion:

We show in this paper that contact guidance fidelity is strongly cell type dependent, where mesenchymal cells contact guide with high fidelity, epithelial cells contact guide with intermediate fidelity and amoeboid cells essentially ignore the contact guidance cue. Others have shown that there are cell type differences in response to contact guidance cues [26–29]. Broadly, these results match what we observe. Fibroblasts and more mesenchymal cells contact guide best, followed by epithelial cells, followed by amoeboid cells. However, many of these previous reports have been conducted on grooves and only specific groove characteristics result in cell-type differences. We have previously shown that aligned collagen fibrils assembled on mica reveal contact guidance differences across cells that are masked in systems like grooves or microcontact printed lines [19]. Furthermore, many of the substrates used to tease out cell type differences were very stiff and the role of stiffness on tuning the contact guidance of different cells was not explored except in one report [29].

In addition to broadly observable cell type differences contact guidance, we demonstrate that stiffness for optimal contact guidance is different for different cell types. Highly contractile cells like HFFs engage in contact guidance that is independent of stiffness. Similarly, amoeboid cell (THP-1) contact guidance is also unaffected by the underlying substrate stiffness. Only cells with intermediate contractile behavior, including MDA-MB-231, WM-266-4 and HaCaT cells show noticeable maxima in directionality index, whereas less contractile cells show optimal contact guidance on stiffer substrates. Substrate stiffness is an appreciated modulator of cell function and likely tunes contact guidance fidelity due to overlapping intracellular mechanisms [44,45]. Previously, we showed subtle differences when the underlying substrate stiffness was altered, but these were only explored in the mesenchymal MDA-MB-231 cells and amoeboid MTLn3 cells [20]. The literature shows conflicting reports examining contact guidance in MDA-MB-231 cells on flexible grooves. One report indicated that increased stiffness diminishes the cell aspect ratio [34], suggesting that that contact guidance decreases under stiffer conditions, however another report showed increased elongation and small increases in cell alignment in both MDA-MB-231 cells as well as a more epithelial-like cell line, T47D cells when stiffness was increased [29]. We showed decreases in MDA-MB-231 cell contact guidance in 3D environments after collagen crosslinking leading to increases in stiffness [12], matching what we observed on aligned fibrils in 2D here, suggesting again that the aligned collagen fibril assembled system mimics 3D environments and provides clarity with respect to discrepancies observed when using groove systems. Strengthening this argument is evidence indicating that fibril recruitment, a feature in our system and one that is particularly important soft environments dramatically enhances contact guidance [46]. Interestingly, two reports using fibroblasts and not MDA-MB-231 cells in 3D environments showed that increases in stiffness increase fibroblast contact guidance only modestly,[11,47]. It is not surprising that different cells respond differently

to contact guidance cues and that the response is stiffness-dependent. Fibroblasts must remodel the ECM

while moving along fibrils during wound healing. Since stiffness changes dramatically during the wound

process, but fibroblasts must continue to contact guide and generate traction force, they may need to be

less sensitive to stiffness cues. Similarly, for amoeboid cells, which must randomly sample the wound

environment, it might be important for them to ignore the directional cue. Indeed, aligned collagen fibrils

in the tumor microenvironment do not seem to affect T-cell infiltration [23]. Consequently, tissue

environments with different stiffness are likely to control cells with unique functions differently.

Other interesting behaviors emerged when examining cancer cell-specific responses. Indeed, the

ability of cancer cells to engage in contact guidance correlates with their migration mode. A recent paper

has shown that the strongest response to contact guidance cues occurs in cells that have processed through

the epithelial-to-mesenchymal transition (EMT), followed by epithelial cells, while amoeboid cells

showed the weakest fidelity to these cues, matching our observations [28,32]. However, our results indicate

that cancer cells, MDA-MB-231 and WM-266-4 cells, show dramatically increased contact guidance

responses on aligned collagen assembled on mica versus aligned collagen transferred to glass. This is in

contrast to non-transformed cells [11,29], which show only a small difference in contact guidance fidelity

when the stiffness of the substrate is changed. We do observe that cancer cells are more sensitive to

stiffness differences, decreasing their contact guidance on flexible substrates as stiffness increases.

However, aligned collagen fibrils assembled on mica do seem to have a unique capability to align cells

even in comparison to aligned collagen fibrils transferred to flexible substrates. As mentioned above,

fibril recruitment to the cell periphery is inhibited even when collagen fibrils are transferred to soft 200 Pa

substrates. Free fibers that can be remodeled and recruited to the cell periphery likely amplify the signal

for contact guidance [20,46]. Our work strengthens the argument that for contact guidance, specific cancer-

related pathways sensitize cancer cells to stiffness in comparison to non-transformed cells. It is known

that cancer cells have distinct mechano-sensitivity when compared to non-transformed cells [48]. This

includes upregulation and expression of mechanosensitive proteins such as Piezo1 [49] as well as the

ability of cancer cells to avoid death and resist inhibitor treatment on soft substrates [50] or alter

metabolism based on the mechanical properties of the ECM [51]. This differential contact guidance

sensitivity to substrate stiffness is yet another differentially regulated mechanical behavior in cancer cells.

We also demonstrate that intracellular contractility is a dominant predictor of contact guidance

behavior. Both myosin phosphorylation and compaction assays revealed a strong correlation between

increased directionality index and elevated contractility. Interestingly, the only dramatic difference

between compaction and myosin phosphorylation levels was WM-266-4 cells. It seems that contractility

better predicts contact guidance on aligned collagen fibrils that are stiff and cannot be remodeled

(collagen fibrils assembled on mica). Myosin phosphorylation is elevated in environments when cells can

recruit fibrils [46], but we assessed myosin phosphorylation on tissue culture plastic due to the infeasibility

of using western blotting to assess myosin phosphorylation on our aligned collagen fibril substrates

containing a small number of cells compared to that needed for western blotting. This likely explains the

ability of our measures of contractility to track less well with directionality index on collagen fibrils

assembled on mica. We measured myosin phosphorylation using immunofluorescence on collagen fibrils

assembled on mica, but the interpretation can be challenging due to the inability to properly quantify the

signal for dramatically different morphologies. For instance, rounded cells on soft substrates showed the

largest myosin phosphorylation level. Multiple studies underscore the role of contractility in cell

alignment and contact guidance [8,12,16,19,28,29]. While early migration stages are contractility-independent,

later stages require actomyosin traction forces for effective contact guidance [40]. Studies on microcontact-

printed collagen lines further show that MTLn3 cell directionality is diminished after blocking

contractility [8]. In a variety of cells, blocking contractility reduced alignment along microgrooves,

weakening contact guidance [28,29]. Similarly, in 3D collagen gels, inhibiting contractility with blebbistatin

or a myosin phosphorylation blocker lowered directionality to levels observed on non-aligned substrates

in MDA-MB-231 cells [12,52]. Taken together myosin contractility is vitally important in contact guidance,

where enhanced myosin contractility leads to high fidelity contact guidance.

In addition to myosin contractility, we established that formins and Arp2/3 modulate contact

guidance in a reciprocal manner. In mesenchymal cells, formin inhibition decreases directionality index

indicating a diminished contact guidance fidelity, whereas Arp2/3 inhibition increases directionality index

indicating an enhanced contact guidance fidelity. Similar behavior is seen in epithelial cell migration,

where formin inhibition diminishes the residence time in parallel migration as well as the fraction of cells

in parallel migration, but increases the fraction of cells in perpendicular migration. Arp 2/3 on the other

hand seems to enhance the fraction of cells that migrate parallel to the aligned collagen. Our motivation

for examining how both formins and Arp2/3 control directionality flows from two observations. First, the

F-actin networks that formins and Arp2/3 create are distinct in nature. Formins generate linear F-actin

structures like various forms of stress fibrils that help the cell form and maintain traction in a particular

direction of migration through stable focal adhesions attached to the ECM. Arp2/3 generates branched F-

actin networks that constitute the lamellipodium, a rounded structure that can also facilitate dynamic

adhesion and can bias migration in a particular direction but has much more plastic control of directional

persistence. Second, it has been elegantly shown in a variety of contexts that G-actin can be limiting, so

diminishing of linear F-actin structures through formin inhibition results in more branched F-actin

structures and vice versa, setting up feedback for reciprocal control by these two distinct F-actin networks

[41,53]. While the reciprocal regulation of contact guidance occurs at high formin (~20 μM) and Arp2/3

(~25 μM) inhibitor concentrations, submaximal concentrations produce results that are difficult to

reconcile. For instance, submaximal formin inhibitor concentrations show enhanced contact guidance and

submaximal Arp2/3 inhibitor concentrations show diminished contact guidance. Future work will be

geared toward understanding these results in the broad context of formin and Arp2/3 regulation. However,

very little work to date has examined the role of formins and Arp2/3 in contact guidance. In 1D contact

guidance systems, where cells are confined to 1D migration only, formins are important, whereas Arp2/3

is dispensable in maintaining speed [36,54,55]. However, these 1D systems dimensionally restrict migration

in a way that does not allow the assessment of how directional fidelity is controlled. In 2D systems of

contact guidance that include microcontact printed lines and ridges, formins seem to play a positive role

in controlling directional fidelity, agreeing with our results [34,37]. On the other hand the role of Arp2/3 is

less clear. Work exploring contact guidance on flexible substrates indicates that inhibiting Arp2/3

diminishes contact guidance [34] whereas other work on stiff substrates indicates that inhibiting Arp2/3

enhances contact guidance [37]. The current work adds evidence to the positive role of formins and the

negative role of Arp2/3 in enhancing contact guidance.

Finally, we have discovered a new mode of migration on aligned collagen fibrils for epithelial

cell migration. On strong contact guidance cues like ridges and lines of ECM, most all cells respond by

migrating parallel to the groove or line direction. As mentioned above our collagen fibril substrates reveal

cell type differences that can be masked in these other systems and these differences map to responses

observed in 3D. This was demonstrated by the difference between migration of mesenchymal cells, which

migrate on collagen fibrils with high fidelity and amoeboid cells, which essentially ignore the collagen

fibril direction. We find that epithelial cells can migrate in both a parallel and perpendicular fashion. This

behavior is only revealed when examining cell migration and is less apparent when examining cell

alignment in fixed images. This appears to be a new phenotype not observed by those examining fixed

cell morphology and one that is more readily observable using our aligned collagen fibril system.

Normally, during wound healing, collective migration occurs resulting in re-epithelialization of the

wound. However, we imagine that in some instances single cells detach or are left during injury. As the

wound develops, they interact with aligned fibrin or collagen fiber networks that are generated by

contractile dermal fibroblasts. It might be crucial for these cells to be somewhat agnostic to the directional

alignment of the collagen, necessitating both parallel and perpendicular migration. Alternatively, this

single-cell multi-directional phenotype might indicate similar collective cell responses on aligned

collagen fibrils that has not yet been observed. Indeed, work has been carried out trying to understand

collective cell migration on contact guidance cues and sheets indeed prefer migration parallel to the

groove, but again, perhaps there are some responses that are masked by these non-fibril systems [56–58].

External signals, such as stiffness, regulate the balance of perpendicular and parallel migration and both

formins and Arp2/3 play similar roles in epithelial cells as they do in mesenchymal cells in facilitating

and inhibiting contact guidance. This may be a single-cell specific phenotype, given that inhibiting

Arp2/3 in collective migration seems to diminish directional persistence in collective sheet migration on

grooves [56]. However, collective migration is intimately tied to cell-cell contacts, which depend on

Arp2/3 and, when disrupted, may negatively impact directional fidelity. How the F-actin structure

dynamically changes during parallel and perpendicular migration as well as how formins and Arp2/3

regulate this behavior differently during each mode of migration is still an open question and will need to

be assessed in the future. The discovery of this additional mode of directional migration likely reveals

important features of the ECM that regulate wound healing and could be encoded into tissue engineered

constructs to facilitate directed migration.

5. Conclusions:

We show that dermal fibroblasts are strong and can delaminate collagen fibrils from the surface of mica unless these fibrils are transferred and covalently attached to other substrates. Mesenchymal cells engage in robust contact guidance, whereas epithelial cells and amoeboid cells contact guide with lower fidelity. Contact guidance is strongly correlated with the contractile ability of cells. Cancer cells are more sensitive to stiffness during contact guidance than non-transformed cells, decreasing their directional fidelity on stiffer substrates. Formins and Arp2/3 reciprocally control contact guidance, where formins facilitate better contact guidance and Arp2/3 facilitates poorer contact guidance. Finally, epithelial cells appear to switch between parallel and perpendicular migration on aligned fibrils. This behavior is stiffness-dependent, where stiffer environments result in better contact guidance at slower rates. Formins enhance the parallel movement, whereas Arp2/3 has a richer control over contact guidance, diminishing parallel migration, but also decreasing perpendicular fraction.

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Data Availability Statement

The data that support the findings of this study are available from the corresponding author upon reasonable request.

Conflict of Interest

The authors declare that there are no conflicts of interest regarding the publication of this manuscript.

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A.F.: Conceived experiments, conducted experiments, analyzed the data and interpreted the data across all figures, prepared the figures, wrote the article and edited the article. S.T.: Wrote code and analyzed the data in **Figures 1-8** and **Supplementary Figures 2-8**. S.A.S.: Conceived experiments, conducted experiments, analyzed the data and interpreted the data in **Figures 3-5** and **Supplementary Figures 3-5**, wrote article and edited the article. F.R.N.: Conceived experiments, conducted experiments, analyzed data and interpreted the data in **Figure 3** and **Supplementary Figure 3**, wrote article and edited the article. I.C.S.: Conceived experiments, analyzed the data and interpreted the data across all figures, wrote the article, prepared the figures and edited the article.

Figure 1: Contractile fibroblasts respond differently on different collagen substrates. (**A**) AFM

image of collagen assembled on mica. AFM scale bar is 1 μm. Live-cell phase contrast microscopy

images of HFFs on mica at 0, 2, and 4 h. Phase contrast image scale bar is 150 μm. (**B**) Fraction of initial

cells remaining on the mica surface over time as assessed after fixation. $N_{samples} \geq 4$, $N_{cells} \geq 265$ and N_{images}

≥ 15 (**C**) Various collagen patterns assembled on mica under different conditions. Trimers (t): citric acid

buffer (pH 4.3) with 200 mM KCl, 10 μg/ml collagen and a 12 hours incubation. Aligned fibrils (af): 50

mM Tris buffer (pH 9.2) with 200 mM KCl, 10 μg/ml collagen and a 12 hours incubation. Multi-

directional fibrils (mdf): 50 mM Tris buffer (pH 9.2) with 200 mM KCl, 100 μg/ml collagen and a 12

hours incubation. Transferred fibrils (tf): 50 mM Tris buffer (pH 9.2) with 200 mM KCl, 10 μg/ml

collagen, a 12 hour incubation and transferred onto functionalized glass. Scale bar is 1 μm. (**D**) Phalloidin

staining showing F-actin structure and HFF morphology on collagen fibrils under the same conditions as

in C. Scale bar is 150 μm. (**E**) Directionality index of HFFs on different collagen patterns and after

different incubation times on the collagen fibrils. $N_{samples} \geq 2$ and $N_{cells} \geq 122$. Error bars are 95%

confidence intervals.

Figure 2: Different cells spread and align to different extents on aligned collagen fibrils. (**A**) F-actin staining of cells on both mica (top) and glass (bottom). Scale bar is 200 μm. (**B**) High resolution of F-actin and paxillin staining of cells on glass. Scale bars are 25 μm. Cell (**C**) area ($N_{samples} \geq 2$ and $N_{cells} \geq$ 152) and (**D**) Directionality index ($N_{samples} \geq 2$ and $N_{cells} \geq 122$) of different cell lines plated on collagen fibrils on mica (open bars) or those transferred to glass (solid bars). Error bars represent 95% confidence intervals.

Figure 3: Higher contractile cells engage in optimal contact guidance at lower stiffness. (**A**)

Directionality index of various cell lines on different substrates, including 0.2 kPa PAA (0.2), mica (m), 2

kPa PAA (2), 20 kPa PAA (20) and glass (g). $N_{samples} = 2$ and $N_{cells} = 122$. (**B**) F-actin (green) and

phosphomyosin (pMyo, red) localization in MDA-MB-231 cells on 0.2 kPa PAA gel with transferred

fibrils, glass (g) with transferred fibrils, mica (m) with aligned fibrils, and glass (g) with deposited

collagen trimers. The scale bar is 25 μm. (**C**) Phosphorylated myosin (pMyo) intensity in

immunofluorescence images of fixed MDA-MB-231 cells on various substrates, including 0.2 kPa PAA

gel (0.2), mica (m), 2 kPa PAA (2), 20 kPa PAA (20), and glass (g) with both collagen fibrils (solid bars)

and trimers (open bars), $N_{samples} \geq 2$ and $N_{cells} \geq 28$. (**D**) Phosphorylated myosin (pMyo) intensity from

western blots. $N_{samples} \geq 2$. (**E**) Fractional compaction calculated from initial and 48 hours diameters of

collagen gels across all cell lines. $N_{samples} \geq 3$. Error bars represent 95% confidence intervals.

Figure 4: Formins inhibition marginally disrupts mesenchymal cell alignment and collagen fibril delamination, but dramatically diminishes gel compaction. (**A**) Immunofluorescence images of F-actin localization in HFF and MDA-MB-231 cells treated with 0.1% DMSO, 20 μM SMIFH2 and 50 μM SMIFH2 on both mica (m) and glass (g) substrates. The scale bar is 100 μm. (**B**) Directionality index of HFF cells treated with varying concentrations of SMIFH2 on glass (g) substrates, $N_{samples} \geq 3$ and $N_{cells} \geq$ 708. The open circles at 0 μM SMIFH2 are cells without any treatment and the solid circles are cells treated with 0.1% DMSO. (**C**) Directionality index of MDA-MB-231 cells treated with different concentrations of SMIFH2 on both mica (m) and glass (g) substrates, $N_{samples} \geq 1$ and $N_{cells} \geq 53$. (**D**) Fraction of initial HFF cells treated with and without 20 μM SMIFH2 remaining on the mica surface over time as assessed after fixation, $N_{samples} \geq 4$, $N_{cells} \geq 265$ and $N_{images} \geq 15$ (**E**) Fractional compaction of HFF cells treated with different concentrations of SMIFH2 calculated from initial and 48 hour diameters of collagen gels, $N_{samples} \geq 3$. Error bars represent 95% confidence intervals.

Figure 5: Arp2/3 inhibition enhances mesenchymal cell alignment, but does not robustly affect collagen fibril delamination or collagen gel compaction. (**A**) Immunofluorescence images of F-actin localization in HFF cells treated with 5 µM and 25 µM of CK-666 fixed on glass (g). The scale bar is 100 µm. (**B**) Directionality index of fixed HFF cells on glass substrates as a function of CK-666 concentration including 5 and 25 µM CK-666. The open circles at 0 µM SMIFH2 are cells without any treatment and the solid circles are cells treated with 0.1% DMSO, $N_{samples} \geq 3$ and $N_{cells} \geq 594$ (**C**) Fraction of initial HFF cells treated with or without 5 µM CK-666 remaining on the mica surface over time as assessed after fixation, $N_{samples} \geq 4$, $N_{cells} \geq 256$ and $N_{images} \geq 15$. (**D**) Fractional compaction of HFF cells treated with different concentrations of CK-666 calculated from initial and 48 h diameters of collagen gels across all cell lines, $N_{samples} \geq 3$. Error bars represent 95% confidence intervals.

Figure 6: Epithelial cells exhibit both parallel and perpendicular movement that generates low directionality. (**A**) Phase contrast, live cell migration montages of HaCaT cells on different substrates: mica (m), 2 kPa PAA (2), and glass (g). Circles and squares mark previous cell positions. The collagen fibril direction is denoted with the white arrow (col θ). The scale bar is 50 μm. (**B**) Directionality index and (**C**) cell speed, fixed cells: $N_{samples} \geq 3$ and $N_{cells} \geq 483$, and live cells: $N_{samples} \geq 4$ and $N_{cells} \geq 41$. (**D**) Residence time, indicating the duration cells spend in parallel or perpendicular migration with respect to collagen fibrils and (**E**) fraction of migration steps taken by cells in parallel and perpendicular directions relative to collagen fibrils, $N_{samples} \geq 4$ and $N_{cells} \geq 41$. Error bars represent 95% confidence intervals.

Figure 7: In epithelial cells Arp2/3 inhibition increases parallel and perpendicular migration,

whereas formins inhibition increases perpendicular migration only. (A) immunofluorescence images

of HaCaT cells fixed on glass treated with 0.1% DMSO, 20 μM SMIFH2 and 25 μM CK-666. Scale bar is

50μm (**B**) Live cell migration montages of HaCaT cells on glass without inhibitors, with 20 μM SMIFH2

and with 25 μM CK-666. Scale bar is 50 μm (**C**) Directionality index of both fixed $N_{samples} \geq 4$ and $N_{cells} \geq$

712 and live cells $.N_{samples} \geq 5$ and $N_{cells} \geq 85$ under different conditions: no inhibitor, 20 μM SMIFH2 and

25 μM CK-666. (**D**) Cell speed calculated from live cell migration under the same conditions: no

inhibitor, 20 μM SMIFH2 and 25 μM CK-666, $N_{samples} \geq 5$ and $N_{cells} \geq 85$ (**E**) Average residence time of

cells moving parallel (less than 30° deviation) or perpendicular (more than 60° deviation) to collagen

fibrils. $N_{samples} \geq 5$ and $N_{cells} \geq 85$ (**F**) Fraction of cells moving parallel (deviation less than 30°) or

perpendicular (deviation more than 60°) to collagen fibrils. $N_{samples} \geq 5$ and $N_{cells} \geq 85$.

Figure 8: Epithelial cells demonstrate a biphasic dependence of speed on directionality in response

to a variety of stiffness and F-actin regulatory protein inhibitors. The speed and directionality index

calculated from live cell migration of HaCaT Cell on various conditions. $N_{samples} \geq 4$ and $N_{cells} \geq 41$ and

error bars represent 95% confidence intervals.