Embedding muscle fibers in hydrogel improves viability and preserves contractile function during prolonged *ex vivo* culture

Running Title: *Ex vivo* culture of FDB muscle fibers

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Author contributions: LAV, OE, CACO, TJK designed the study. LAV and OE were responsible for isolation of muscle fibers. LAV, OE, DH and RMNB performed the experiments in the laboratory and were responsible for data collection. LAV performed statistical analyses and created figures. LAV and OE drafted the manuscript. LAV, OE, CACO, and TJK critically revised the manuscript. All authors read and approved the manuscript.

Funding: This work was supported by internal funding from the Department of Physiology (T.J.K) and a research grant from A Foundation Building Strength for Nemaline Myopathies and from Prinses Beatrix Spierfonds (W.OR23-06) (CACO).

Summary

In this work, the authors demonstrate that a low-serum, 3D *ex vivo* culture model preserves muscle fiber viability and contractility while reducing dedifferentiation. This model system can be utilized to conduct prolonged *ex vivo* pharmacological or genetic interventions to study fundamental muscle fiber processes or disease mechanisms.

Abstract

Ex vivo culture of isolated muscle fibers can serve as an important model for *in vitro* research on mature skeletal muscle fibers. Nevertheless, this model has limitations for long-term studies due to structural loss and dedifferentiation following prolonged culture periods. This study aimed to investigate how *ex vivo* culture affects muscle fiber contraction and to improve the culture system to preserve muscle fiber morphology and sarcomere function. Additionally, we sought to determine which culture-induced changes can negatively affect muscle fiber contraction. We cultured isolated flexor digitorum brevis (FDB) muscle fibers in several conditions for up to 7 days, and investigated viability, morphology, the unloaded sarcomere shortening in intact fibers, along with force generation in permeabilized muscle fibers. In addition, we examined changes to the microtubule network. We found a time-dependent decrease in contractility and viability in muscle fibers cultured for 7 days in a 2D environment. Conversely, we found that culturing FDB muscle fibers in a low-serum, 3D culture environment reduces markers of muscle fiber dedifferentiation (i.e. sprouting), improves viability and retains contractility over time. We discovered that the loss of contractility of cultured muscle fibers was not the direct result of reduced sarcomere function but could be partially explained by changes to the microtubule network. Collectively, our findings highlight the importance of providing muscle fibers with a 3D environment during *ex vivo* culture, particularly when testing pharmacological or genetic interventions to study viability or contractile function.

Introduction

Skeletal muscle tissue is essential for both metabolic and mechanical functions (Kim et al., 2016, Frontera and Ochala, 2015, McCuller et al., 2024, Argiles et al., 2016), including the storage and consumption of amino acids (Aguirre et al., 2013, Argiles et al., 2016) and glucose (Sylow et al., 2017), endocrine activities (Pedersen and Febbraio, 2008, Pedersen and Febbraio, 2012), protecting vital organs, and enabling locomotion through coordinated contraction of muscle fibers (Frontera and Ochala, 2015, McCuller et al., 2024, Schnyder and Handschin, 2015). These diverse functions are facilitated by the hierarchical organization of muscles, which consists of muscle fibers, myofibrils, and sarcomeres (Frontera and Ochala, 2015). Sarcomeres, the smallest contractile units, are arranged in series to form myofibrils (Frontera and Ochala, 2015, McCuller et al., 2024), which contribute to the characteristic striated appearance of muscle tissue. Myofibrils are further organized into muscle fibers, large multinucleated cylindrical cells extending from tendon to tendon, whose contraction enables the function of skeletal muscle (Frontera and Ochala, 2015, Gotti et al., 2020). The ability of the muscle fiber to produce contractile force depends on achieving and maintaining this hierarchical organization.

In muscle research, *in vitro* muscle fiber culture has been used due to its simplicity, access to unlimited biological material, and reduced need for laboratory animals (Khodabukus et al., 2018, Guo et al., 2014, Verma et al., 2020). Common models include the culture of primary cells (Roman et al., 2018), immortalized cell lines (Denes et al., 2019), or induced pluripotent stem cell (iPSC)-derived myoblasts (Bou Akar et al., 2024) and the subsequent differentiation into immature myotubes. However, these models often fail to replicate the complex architecture of muscle fibers (Khodabukus et al., 2018, Smith and Meyer, 2020), as differentiated myotubes often lack defining features such as a large cross-sectional area (CSA) (Khodabukus et al., 2018, Smith and Meyer, 2020), organized cytoskeleton network (Khodabukus et al., 2018, Smith and Meyer, 2020, Engler et al., 2004), proper alignment of sarcomeres (Engler et al., 2004) in series and parallel, mature sarcomere proteins (Ravenscroft et al., 2007), fiber type variations (Khodabukus et al., 2018), and junctional regions (Khodabukus et al., 2018, Smith and Meyer, 2020). In particular, *in vitro* studies are limited if the primary outcome is assessing differences in contractile function, thus limiting the ability to translate findings into an *in vivo* context.

Ex vivo fiber culture is a viable alternative to traditional methods (Stange et al., 2020, Duddy et al., 2011). In this approach, muscle fibers fully mature *in vivo* before the entire muscle is enzymatically digested to obtain single muscle fibers (Smith and Meyer, 2020, Stange et al., 2020, Duddy et al., 2011, Pegoli et al., 2020). This approach yields hundreds of viable and intact muscle fibers with preserved sarcomere contraction and cellular integrity, making them suitable for contraction-based studies (Garcia-Pelagio et al., 2020, Keire et al., 2013). Despite the potential of *ex vivo* cultures, isolated muscle fibers exhibit limited viability, with rapid deterioration depending on the culture conditions (Keire et al., 2013, Smith and Meyer, 2020). Studies focused on the serum content of culture media showed that high serum content (10-20%) has a detrimental effect on muscle fiber morphology and health by promoting the proliferation of satellite cells and dedifferentiation of muscle fibers, while low to serum-free conditions limited satellite cell proliferation, and dedifferentiation of muscle fibers (Renzini et al., 2018, Selvin et al., 2015, Rosenblatt et al., 1995, Brown and Schneider, 2002). Using such media compositions, fibers can only be cultured in suspension for up to 3-4 days (Smith and Meyer, 2020, Renzini et al., 2018) unless adhesion is promoted using laminin-coated dishes (Pasut et al., 2013, Guo et al., 2014, Smith and Meyer, 2020, Renzini et al., 2018). Although modulating serum content and promoting adhesion can improve the longevity of muscle fiber culture, these interventions are not enough to preserve muscle fiber morphology for longer than 12 days (Brown and Schneider, 2002).

Long-term studies on *ex vivo* muscle fibers are difficult, and most studies using this model focus on short-term interventions like drug testing (Hoppstadter et al., 2020), or satellite cell activation and muscle fiber regeneration (Brun et al., 2018, Renzini et al., 2018, Feige et al., 2021). The handful of studies that make use of long-term *ex vivo* muscle fiber culture focused on muscle fiber morphological alterations (Renzini et al., 2018, Brown and Schneider, 2002, Ravenscroft et al., 2007), without assessing the effect of long-term culture on contractile function. Furthermore, while some protocols for 3D muscle fiber culture exist (Rausch et al., 2020, Vonk et al., 2023), their effects on contractile performance in both long- and short-term studies remain largely unknown. The development of a long-term culture system that maintains muscle fiber contraction would allow for contraction-based studies at the single-cell level. These include investigations into muscle fiber wasting, the effects of extended pharmacological treatments, and systematic interventions through genetic manipulation using viral approaches.

In this study, we aimed to characterize the contractile function of muscle fibers during prolonged culture, and to optimize culturing conditions for muscle fibers to extend their viability while preserving contractile function. We first validated culture medium composition and assessed morphological and functional changes in a 2D culture setup over a longer culture time. We then tested the effect of embedding cells in a fibrin-based hydrogel to mimic the native environment of a muscle fiber. By evaluating fiber morphology, contractility, and sarcomere structure, we investigated the impact of culture duration on *ex vivo* muscle fibers, comparing 2D and 3D conditions. Finally, we aimed to identify factors driving muscle fiber deterioration in culture, which could be modulated to preserve muscle fiber function during prolonged *ex vivo* culture. Our main findings show that muscle fiber function and viability deteriorate over time in culture, and that culturing muscle fibers in fibrin-based hydrogel improves viability and contractile function. We further reveal that culture induces changes to the microtubule network, and that the microtubule network plays an important role in muscle fiber contractile dynamics.

Methods

Muscle fiber isolation

Post-mortem tissue was obtained from animals sacrificed for other approved research projects and/or breeding surplus of the VU University in accordance with the European Council Directive (2010/63/ EU) by permission of the Animal Research Law of the Netherlands. Isolated mature single muscle fibers were obtained following the protocol described by Vonk et al. (2023). Briefly, adult wild-type C57BL/6 mice from a broad range of genetic backgrounds were obtained from the Amsterdam Animal Research Centre. Whole flexor digitorum brevis (FDB) muscles were dissected from the mouse by cutting the tendons. Muscles were transferred to pre-warmed (37°C) and pH equilibrated (5% CO_2) dissection medium, consisting of Minimum Essential Medium (MEM) with high glucose and pyruvate (Gibco, Thermo Fisher), 10% heat-inactivated fetal bovine serum (FBS, Thermo Fisher) and 1% penicillin-streptomycin (Sigma Aldrich). FDB muscles were then transferred to 5ml of sterilized 0.2% collagenase type II (Worthington Biochemicals) dissolved in a dissection medium and digested in a tissue culture incubator at 37°C and 5% CO_2 for 70-80 minutes. After digestion, the whole muscles were carefully transferred to 3ml of dissection medium and incubated for 30 minutes in the same conditions. To release the individual muscle fibers, the digested muscle was triturated using two p1000 pipette tips with bore widths of different sizes. Starting with the tip with the widest opening, the muscles were triturated until all fibers were released and in suspension. The tendons were then carefully removed with a regular pipette tip. Myoblasts and remaining tissue were removed through two rounds of gravity sedimentation.

Muscle fiber culture

Isolated mouse FDB muscle fibers were cultured in a medium consisting of MEM with high glucose and pyruvate (Gibco, Thermo Fisher) supplemented with 0.4% Serum Replacement 2 (50X) (Sigma Aldrich), 1% Horse Serum (Sigma Aldrich) and 1% penicillin/streptomycin (Sigma Aldrich). For 2D fiber cultures, culture plates were coated with mouse laminin (Sigma Merck) diluted in MEM at 1:25 for 2 hours before seeding to allow adhesion to the culture dish.

To test the effects of different serum concentrations on muscle fiber culture health, muscle fibers were cultured for 7 days in medium of differing compositions. Tested conditions included serum-free Gibco-MEM, Gibco-MEM supplemented with 0.4 % serum replacement 2 and 1% Horse serum (low serum), and dissection medium containing 10% FBS.

Fibrin hydrogel preparation and seeding

For the 3D culture condition, a hydrogel was formulated in which fibers could be embedded immediately after isolation and prior to putting them in culture. Hydrogels consisted of 2.5, 3.75 or 5 mg/ml fibrin, to which 10% of either 4 mg/mL Matrigel GFR Membrane Matrix (Matrigel, Corning) or 4mg/mL Geltrex LDEV-Free Reduced Growth Factor Basement Membrane Matrix (Geltrex, Thermo Fisher) diluted in Iscove's Modified Dulbecco's Medium + L-glutamine (IMDM, Thermo Fisher) was added.

Fibrinogen isolated from bovine plasma (Sigma Aldrich) was dissolved in phosphate-buffered saline (PBS, Gibco) at a stock concentration of 20 mg/ml. Fibrinogen solution was then filter-sterilized using a 0.2 µm filter (Whatman), and sterile fibrinogen stocks were stored at -80° C. Thrombin isolated from bovine plasma (Sigma Aldrich) was dissolved in PBS at a concentration of 125 U/ml and stored at -20 ^{o}C.

To crosslink fibrin gels, solutions of fibrinogen and thrombin were prepared separately. "Gel solution" consisted of culture medium supplemented with 20% of 4mg/mL Matrigel or Geltrex, and 5-10 mg/ml fibrinogen depending on the final fibrin concentration. "Crosslinking solution" consisted of culture medium supplemented with 60 µM aprotinin and 0.5-1 U/ml thrombin depending on fibrinogen concentration. Both solutions were kept on ice before plating to

prevent premature polymerization of Matrigel or Geltrex. Muscle fibers were seeded in gels by first allowing fibers to settle to the bottom of a 15 ml tube, after which supernatant was removed, and cells were resuspended in crosslinking mix. Fibrin gels were crosslinked by adding equal parts of gel solution to crosslinking solution, mixing briefly, and then transferring to a culture plate dish. Gels were then allowed to solidify at 37 ^{o}C and 5% CO_2 in an incubator for up to 2 hours. After solidification, gels were completely covered with culture medium. When culturing muscle fibers in gel, 60 μM aprotinin and 200 μM tranexamic acid was added to culture medium to prevent degradation of the fibrin gel.

Muscle fiber viability classification

Culture well plates were sampled at 5 random locations for each condition using a ZOE Fluorescent Cell Imager (BioRad) with a 20X objective. Single fiber images were then randomized and presented to 11 participants blinded to the experimental conditions. Participants were asked to classify fiber images according to two predetermined groups: a) Living fibers and b) hypercontracted (HC). An example image of representative fibers was shown during classification. Classification of each fiber was then recorded as the majority vote out of all 11 participants.

Electrical stimulation and contractile measurements

Muscle fibers were stimulated using a 6-well C-Dish insert designed for Corning 24-wells plates (IonOptix) coupled to a Myopacer cell stimulator (IonOptix). Electrical stimulations were performed using bipolar pulses at 10V, a frequency of 1 Hz and a pulse duration of 4 ms. Muscle fiber contractions were then measured by stimulating fibers inside a CytoCypher MultiCell High-Throughput System (IonOptix). Using the CytoSolver software, sarcomere lengths were measured during contractions. From these measurements a contraction transient is generated, recording parameters such as sarcomere length, contractile velocity and contraction duration. Data from each fiber is based on the average of 9-10 subsequent contractions. Automatic data analysis was performed using CytoSolver Transient Analysis Tool software. CytoSolver software automatically excludes single transients that have insufficient $R^2 < 0.95$ fit values. For measurements where transients were rejected by the software, a cut-off of at least 4 transients was maintained, and data points whose average was based on 3 or less transients was removed from the dataset. Muscle fiber contractile parameters recorded by the MultiCell system were the following: Sarcomere length at rest, contractile velocity, contraction duration, % of sarcomere shortening, relaxation velocity, relaxation duration and sarcomere length at peak contraction.

Muscle fiber adhesion contractile measurements

The effects of adhesion during culture were tested by either culturing muscle fibers in 2D as described above, or by free-floating culture using uncoated glass bottom culture plates with laminin. A third condition was also included in which muscle fibers were cultured in 2D for 6 days and dissociated from the culture plate by treatment with 0.25% Trypsin in EDTA (Gibco, Thermo Fischer) for 2 minutes before replating on laminin-coated dishes. All measurements were performed on day 7 post-isolation.

Microtubule network manipulation

To alter the microtubule network, cells were treated with 20 μM Nocodazole (Cayman Chemical) for 2h to depolymerize microtubules or 100 nM Taxol (Cayman Chemical) overnight to stabilize microtubules prior to measurements. The interference with the microtubule network was confirmed through visual inspection via immunofluorescent labeling for α-tubulin.

Immunofluorescent staining and image acquisition

Muscle fibers were fixed by replacing half of the culture medium with a solution of 4% Paraformaldehyde (PFA, Thermo Fischer) for 5 minutes, and then a full replacement with 4% PFA for 10 minutes. PFA was washed out 3 x for 5 minutes with PBS and stored for up to 7 days at 4°C. Samples were then blocked and permeabilized using a blocking buffer solution containing 3% bovine serum albumin (BSA, Sigma Aldrich), 0.2% Triton-X100 (Sigma Aldrich) and 0.05% Tween (Sigma Aldrich) dissolved in PBS for 1 hour at 4°C on a shaker. Samples were then incubated in a blocking solution with added primary antibodies (diluted according to manufacturer's instructions, Table 1) overnight at 4°C on a shaker. Samples were then washed with IF buffer containing 0.3% BSA, 0.2% Triton-X100 and 0.05% Tween dissolved in PBS and incubated with a 1:250 dilution of selected AlexaFluor secondary antibodies, 1:1000 DAPI (Invitrogen) and 1:1000 AlexaFluor Plus 647 Phalloidin (Invitrogen). The excess staining solution was washed out using PBS and samples were stored for up to 5 days in PBS at 4°C. Using a confocal microscope (Nikon Ti2 ZDrive), camera (Prime BSI express, A21A726014), CrestOptics X-Light spinning disc with pinhole 50µm (CrEST X-Light V3), laserbox (NIDAQ AOTF Multilaser) with line wavelengths of 405nm, 470nm, and 555nm, the muscle fibers were imaged at a magnification of 60X (PLAN APO 60X IOL OFN25 DIC) on a confocal microscope. 1 µm Z-stacks of fibers were collected and stacked together using ImageJ to generate maximum-intensity projection images.

Tracking of muscle fiber morphology over time

To determine muscle fiber width, length and sarcomere length changes, muscle fibers were cultured for up to 7 days and images of the same fiber were collected at days 1 and 7. Measurements were performed using ImageJ software. Sarcomere lengths were measured by measuring 10 sarcomeres and averaging sarcomere length over these 10 sarcomeres. For width and sarcomere length measurements, measurements were taken in three locations and averaged to generate a mean per fiber. Width measurements were further normalized to the percentual decrease in sarcomere length of the corresponding fiber, since a decrease in sarcomere length would increase fiber width proportionally.

Permeabilized muscle fiber contraction

We adapted previously described methods for single muscle fiber force measurements (de Winter et al., 2020) to investigate cultured FDB muscle fiber force production after culture. In brief, FDB fibers were cultured in 2D or 3D, for 1 and 7 days. Muscle fibers were first treated with 10 µM N-Benzyl-p-toluenesulfonamide (BTS, Thermo Fisher) for 10 minutes prior to permeabilization, to prevent hypercontraction. Then, culture medium was gradually replaced with skinning solution by three 1:1 media changes. Skinning solution consisted of 50% glycerol (Sigma Aldrich) and 50% relaxing solution containing 100mM balanced electrolyte solution (BES, Sigma Aldrich), 6.97mM ethyleneglycoltetraacetic acid (EGTA, Sigma Aldrich), 6.48mM MgCl2 (Sigma-Aldrich), 5.89mM Na2–adenosine triphosphate (ATP, Sigma Aldrich), 40.76mM K-propionate (Sigma Aldrich), 14.5mM creatine phosphate (Sigma Aldrich) supplemented proteinase inhibitors 200 µg/ml Leupeptin (Thermo Fisher), 100 µM L-trans-3-Carboxyoxiran-2-carbonyl-L-leucylagmatine (E-64, Sigma Aldrich), 250 µM phenylmethylsulfonyl fluoride (PMSF, Sigma Aldrich), 1 mM Dithiothreitol (DTT, Sigma Aldrich), and 10 µM BTS. Single muscle fibers were then attached to aluminum clips and measured as described previously in de Winter et al. (2020) (de Winter et al., 2020).

Statistical analysis

Experimental results from muscle fibers were obtained from at least three separate isolations and 3 individual mice, unless otherwise stated. For single fiber experiments, *n* is denoted as the number of fibers, while *N* is denoted as the number of mice. Mean values were generated for each mouse and statistical analysis was performed using the mean value of each mouse. Statistical analysis tests used were either student's *t*-tests (for datasets with only two conditions), ordinary one-way ANOVA test (for datasets with more than two conditions) with a

Tukey post-hoc test, or two-way ANOVA (for grouped datasets) with a Šidák post-hoc test. Statistical analysis of classification results (percentages) was performed using a Chi-square test on pooled data. All statistical analysis was performed using GraphPad Prism.

Table 1: Antibodies used for Immunofluorescent staining

AB Ref name	**Antigen**	**Antibody isotype**	**Dilution**	**Company**
A7811	α-actinin	MIgG1	1:1000	Sigma Aldrich
A4.1025	Myosin	MIgG2a	1 µg/mL	Developmental Systems Hybridoma Bank
12G10 anti-alpha-tubulin	α-tubulin	MIgG1	1 µg/mL	Developmental Systems Hybridoma Bank
IIH6 C4	α-Dystroglycan	MIgM	1 µg/mL	Developmental Systems Hybridoma Bank

Results

Isolated FDB muscle fibers atrophy, dedifferentiate, and lose contractile function during ex vivo culture in 2D

The culture of *ex vivo* muscle fibers is known to be limited because muscle fibers undergo structural and morphological changes during culture (Smith and Meyer, 2020, Renzini et al., 2018). In this study, we sought to elucidate how muscle fiber morphology and function are affected in a 2D culture setting. To determine changes in muscle fibers during long-term culture, we isolated FDB muscle fibers and cultured them for up to 7 days (**Fig. 1A**). First, we investigated the morphological changes by staining for α-actinin, myosin and nuclei on Days 1 and 7, which revealed sarcomeric aberrations and spreading of fiber ends following 7 days of *ex vivo* culture (**Fig. 1B**), consistent with muscle fiber dedifferentiation (Brown and Schneider, 2002).

Muscle inactivity is known to cause muscle fiber atrophy and loss of function (Sayed et al., 2023). In our experimental setup, isolated muscle fibers are not stimulated during the culture period and thus stay inactive for the duration. To assess if skeletal muscle fibers may atrophy in culture, individual muscle fibers were tracked over 7 days, and their subsequent muscle fiber length and width were measured on Days 1 and 7 post-isolation. Although not significant, our measurements revealed a downward trend in muscle fiber length of ~5% following 7 days in culture (**Fig. 1C**). Conversely, normalized muscle fiber width significantly decreased by ~15% following 7 days of culture (**Fig. 1D**). To determine if long-term culture affected contractile function, we measured unloaded sarcomere shortening and contraction kinetics in response to electrical stimulation at Days 1 and 7 post isolation. We observed a ~5% reduction in resting sarcomere length, going from 1.95 µm on Day 1 to 1.85 µm on Day 7 (**Fig. 1E**). Similarly, sarcomere shortening dropped by ~50% over 7 days of the culture period (**Fig. 1F**). Lastly, contractile velocity declined by ~60% over 7 days (**Fig. 1G**). Taken together, these findings reveal that isolated muscle fibers atrophy and their morphology changes when cultured in 2D for 7 days, in which loss in muscle fiber width is more pronounced than its loss in length. In addition, these changes were accompanied by a significant decline in resting sarcomere length, sarcomere contraction, and contractile velocity.

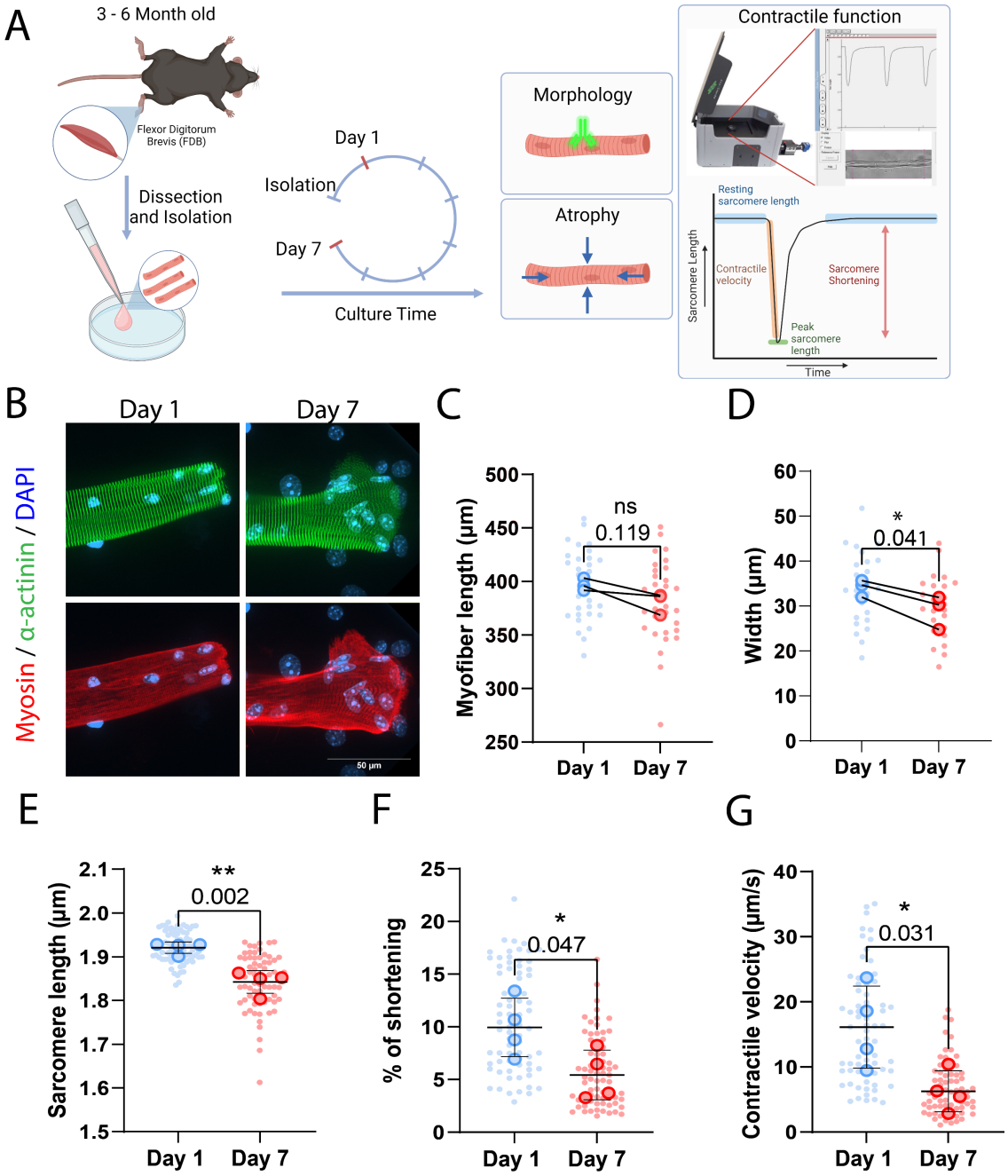

Figure 1: Effects of culture time on muscle fiber morphology and function. (A): Graphical overview of the culture experiment (Image made in Biorender®). (B): Representative confocal maximum intensity projection images taken with a 60x objective stained for α-actinin (green), myosin (red) and nuclei (blue) in muscle fibers cultured at Day 1 and 7. Note the disordered sarcomere structure and spreading of the end of the fiber at Day 7. (C): Muscle fiber length at Day 1 and Day 7 of culture. (D): Muscle fiber width at Day 1 and Day 7 of culture. (E-G): Contractile measurements of muscle fibers kept in culture for 1 and 7 days. (E): Quantification of muscle fiber resting sarcomere length at days 1 and 7 of *ex vivo* culture. (F): Quantification of the percentage of sarcomere shortening at days 1 and 7 of *ex vivo* culture. (G): Quantification of the contractile velocity of muscle fiber at days 1 and 7 of *ex vivo* culture. Data are means ± SEM; N = 3-4 mice and n = fiber. Significance was determined using student's t-test with $p < 0.05$ considered significant with * = $p < 0.05$ and ** = $p < 0.01$.

Low-serum conditions prevent dedifferentiation

To improve the useability of *ex vivo* cultured muscle fibers for long-term experiments, we aimed to prevent morphological alteration and preserve sarcomeric contraction. To do so, we first focused on the culture media composition, since high-serum media has previously been linked to muscle fiber dedifferentiation (Renzini et al., 2018, Selvin et al., 2015, Rosenblatt et al., 1995, Brown and Schneider, 2002). We compared low-serum culture medium to serum-free and high serum (10% FBS) and evaluated their effects on muscle fiber morphology and contractile function. Microscopy imaging of high serum cultures showed complete overgrowth of mononucleated secondary cell types, likely myogenic and fibrogenic cells (**Fig. S1A**), and pronounced dedifferentiation (sarcomeric aberration and branching), especially at the muscle fiber tip as compared to the low serum condition (**Fig. 1A**) and serum-free conditions (**Fig. S1A**). Low serum and serum-free conditions showed less morphological alterations, in which slightly more spreading of the fiber ends was observed in low serum culture. Next, contractile measurements revealed a significant decline in resting sarcomere length in fibers cultured for 7 days in high serum as compared to low and serum-free conditions. To our surprise, this decline in resting sarcomere length did not affect the sarcomere shortening at Day 7 (**Fig. S1C**). Our results support previous findings that high serum induces fiber dedifferentiation (Renzini et al., 2018, Selvin et al., 2015, Rosenblatt et al., 1995, Brown and Schneider, 2002), whereas low-serum medium maintains sarcomere function similarly to serum free conditions. Additionally, our findings suggest that apart from a lowered sarcomere length, the previously observed reduction in contractile function is not directly related to dedifferentiation of the fiber. Because low serum culture did not reduce sarcomere function compared to serum-free culture, we continued with low serum medium for future experiments since it provides essential hormones, lipids and trace elements that may be essential for muscle fiber function.

Embedding muscle fibers in fibrin hydrogel increases viability, reduces dedifferentiation, and partially rescues contractile function

In their native environment, muscle fibers are densely packed and surrounded by an extracellular matrix (ECM) that functions as a supportive scaffold and provides mechanical cues (Purslow, 2002, Engler et al., 2006, Meyer and Lieber, 2011). During the isolation procedure, muscle fibers are removed from their ECM, leaving isolated fibers completely unloaded in the current 2D culture setup. The absence of ECM support and subsequent mechanical forces acting on the cell may induce morphological changes and atrophy of the fibers, leading to the deterioration of muscle fiber contraction. To determine the effect of the ECM on muscle fiber morphology and sarcomere contraction, we compared 2D cultured muscle fibers with those cultured in 3D hydrogels. Hydrogels have unique biomimetic properties and tunable mechanical properties dependent on the polymer-type, polymer concentration, and cross-linking density that can help mimic the micro-environment of cells (Kopecek, 2007, Lin and Anseth, 2009). Thus, we developed a hydrogel matrix to embed fibers during culture and provide a 3D environment. This hydrogel was adapted from muscle tissue engineering protocols, which often use a mix of fibrin and basement membrane matrix solution (van der Wal et al., 2023, Rao et al., 2018). In this formulation, the fibrin supplies most of the structural support, while the added basement membrane matrix may help to facilitate connections between the fiber and the matrix (**Fig. 2A**). First, we tested gels with increasing fibrin concentrations (2.5, 3.75, and 5 mg/ml fibrin) to determine if the cross-linking density would influence muscle fiber contractility, since a higher polymer concentration increases cross-linking density, resulting in a stiffer gel (Lin and Anseth, 2009). Fibrin concentrations did not negatively impact resting sarcomere length (**Fig. S2A**) or contraction of embedded fibers (**Fig. S2B**). Although not significant, a concentration of 5 mg/ml did seem to have a trend toward reducing contractile speed (**Fig. S2C**). Based on these results, it was evident that any of the three fibrin gels could be used without affecting contraction parameters. To simplify the

gel casting procedure, prevent pre-mature solidification of hydrogels, and reduce starting material, we selected the 2.5 mg/ml fibrin concentration for the subsequent 3D experiments.

To explore if this 3D culture environment could improve the viability of isolated skeletal muscle fibers, we first assessed muscle fiber viability through blinded visual classification of cultured muscle fibers according to a representative image (**Fig. 2B**). Results of fiber classification on Day 1 show no significant change in the ratio of live/dead fibers between 2D and 3D (**Fig. 2C**). Over time, we found that culture in 3D significantly increased the ratio of live/dead muscle fibers, indicating a 3D environment promotes increased viability of muscle fibers in culture (**Fig. 2C**).

Next, we focused on the sarcomere structure of muscle fibers by staining for α-actinin, myosin heavy chain, and nuclei after 7 days of culture in either 2D or 3D conditions (**Fig. 2D**). Notably, muscle fibers cultured in 3D lack any of the dedifferentiation (i.e. sprouting) and associated sarcomere disorganization at fiber ends that we observed in our 2D culture (**Fig. 1B**). Like in 2D (**Fig. 1**), we tracked single fibers cultured in 3D and measured their length (**Fig. 2E**) and width (**Fig. 2F**) at Days 1 and 7. Here, we found no significant change in fiber length (**Fig. 2E**). Similar to the 2D culture condition, fiber length exhibited a trend towards shorter muscle fiber length (**Fig. 1C**). Normalized muscle fiber width was significantly decreased in 3D cultured muscle fibers (**Fig. 2F**) similarly to the muscle fibers cultured in 2D (**Fig. 1D**).

Lastly, we compared contractile parameters of muscle fibers kept in 2D and 3D culture conditions to assess how a 3D environment affects contractile function over time. On Day 1, 3D culture had no significant acute effect on contractile function compared to 2D, indicating that any day 7 changes should result from the culture condition alone (**Fig. 2G-I**). Over 7 days of culture, contractile function declined across all parameters in both 2D and 3D cultured fibers, with Day 7 showing significant differences in resting length, sarcomere shortening and contraction speed (**Fig. 2G-I**). Resting sarcomere lengths were noticeably more reduced in muscle fibers cultured in 3D than those in 2D in Multicell measurements (**Fig. 2G**). Conversely, this decrease in sarcomere length was not observed in the experiments where the same fiber was tracked over 7 days (**Fig. S3A**). Intriguingly, sarcomere shortening was reduced to a lesser extent in 3D compared to 2D, showing only a 25% decline as compared to a 50% decline in 2D (**Fig. 2H**). Notably, sarcomere length at peak contraction was higher in 2D but decreased in 3D compared to Day 1 (**Fig. S3B**), while contractile speed measurements showed a minor, non-significant improvement in 3D (**Fig. 2I**). Taken together, these results illustrate that a 3D culture environment provides several benefits to muscle fibers. Namely, it improved viability, reduced dedifferentiation, and preserved contractile function.

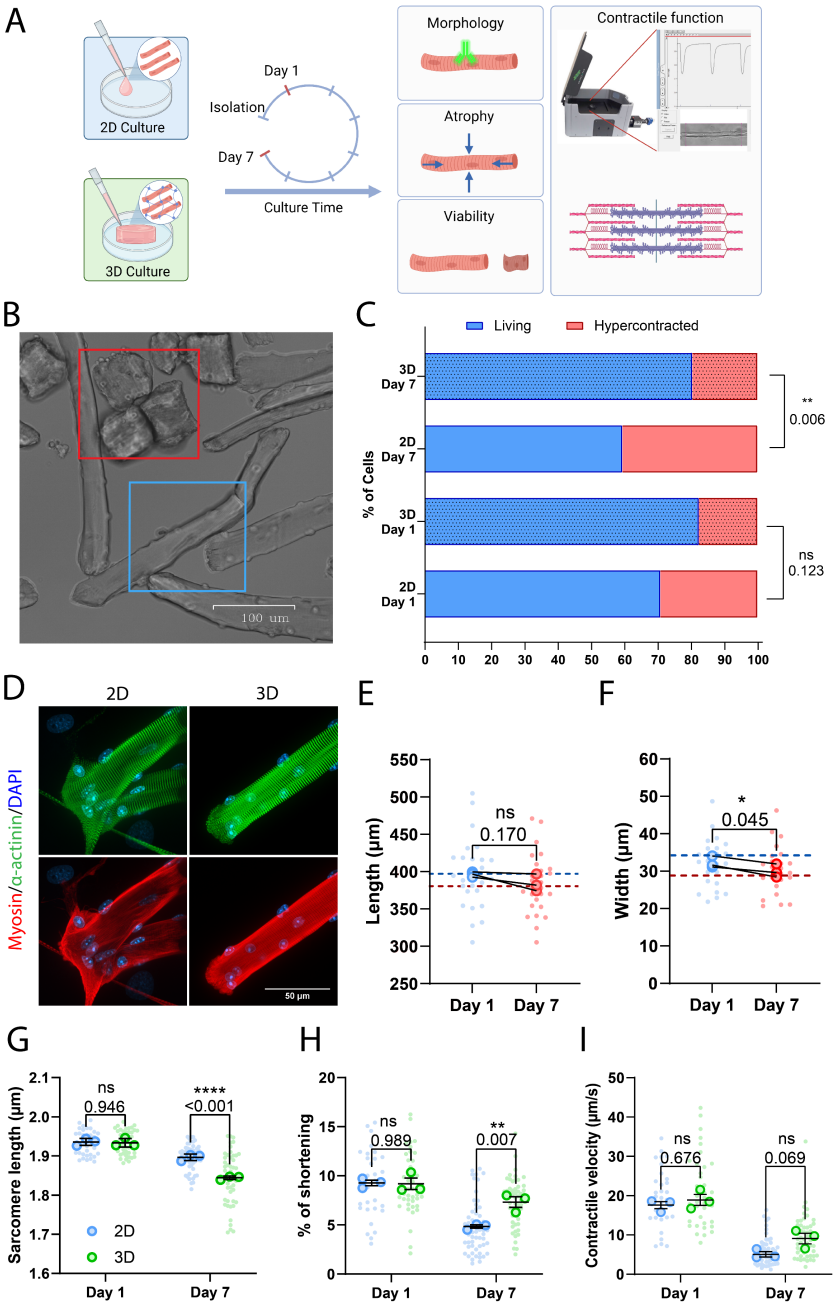

Figure 2: Effects of embedding muscle fibers in a 3D fibrin/basement membrane hydrogel during culture. (A): Graphical illustration of the 3D culture experiment (Image made in Biorender®). (B): Example image used for the classification of muscle fiber viability in which the red box includes dead/hypercontracted muscle fibers and the blue box includes living muscle fibers. (C): Viability classification of muscle fibers cultured in 2D and 3D, at Day 1 and 7. (D): Representative confocal maximum intensity projection images stained for α-actinin (green), myosin (red) and nuclei (blue) in muscle fibers cultured for 7 days in 2D and 3D. Note the lack of sprouting of the muscle fiber end in the 3D cultured muscle fibers. (E): Quantification of muscle fiber length cultured in 3D at Day 1 and 7 of *ex vivo* culture. Dashed lines represent the mean length results of the 2D experiment in Figure 1. (F): Quantification of muscle fiber width cultured in 3D at Day 1 and 7 of *ex vivo* culture. Dashed lines represent the mean length results of the 2D experiment in Figure 1. (G-I): Contractile measurements of muscle fibers kept in culture for 1 and 7 days in 2D and 3D culture systems. (G): Quantification of resting sarcomere length at Days 1 and 7 cultured in 2D and 3D. (H): Quantification of percentage of sarcomere shortening at Day 1 and 7 cultured in 2D and 3D. (I): Quantification of contractile velocity at Day 1 and 7 cultured in 2D and 3D. Data are means ± SEM; $N = 4$ mice and n = fibers. Significance was determined using Chi-square test in panel B, student's *t*-test in panels E-F, and two-way ANOVA for panels G-I with $p < 0.05$ considered as significant with ** = $p < 0.01$ and **** = $p < 0.001$.

Cultured FDB muscle fibers lose contractile force due to atrophy in both 2D and 3D culture

Our experiments revealed that 3D culture conditions helped maintain the contractile performance of cultured muscle fibers. Since muscle fibers cultured in 2D undergo dedifferentiation, atrophy and a reduction of sarcomere contraction, we hypothesized that the underlying sarcomeric structures become altered or damaged during 2D culture, ultimately impairing their contractile function. To investigate whether the changes in contractile function in cultured muscle fibers were due to damage or alterations to the sarcomere structure, we determined the maximal force-generating capacity in permeabilized FDB muscle fibers after culture. These measurements allowed us directly assess sarcomere function, independent of other factors that may affect contraction, such as calcium handling, membrane excitability and substrate adherence. To do this, muscle fibers were cultured for 1 and 7 days in 2D and 3D, after which fibers were permeabilized with triton-X and attached to a length motor and force transducer. Fibers were stretched to a sarcomere length of 2.5 µm for optimal overlap between the thick and thin filaments, after which calcium-induced (pCa^{2+} of 4.5) sarcomere contraction was initiated (**Fig. 3A**). Absolute maximal isometric force was then measured and normalized to fiber cross-sectional area (CSA). Absolute maximal force of muscle fibers significantly decreased after 7 days of *ex vivo* culture independent of culture condition, in which comparison between 2D and 3D showed no significant effect on force generation of muscle fibers (**Fig. 3B**). Next, muscle fiber CSA was measured. A slight downward trend in CSA was noticeable after 7 days of culture, independent of culture condition (**Fig. 3C**), consistent with data from individual fibers tracked over culture time (**Fig. 1D** and **2F**). After normalizing the force of each muscle fiber to its CSA, no significant difference between Days 1 and 7 was observed, which indicates that the decrease in absolute force may be driven by slight atrophy of the muscle fibers (**Fig. 3D**). Our data suggests that long-term muscle fiber culture does not induce significant structural changes or damage to the sarcomere in both the 2D and 3D conditions. Thus, the preserved sarcomere contraction in 3D cannot be explained by direct effects on sarcomere function.

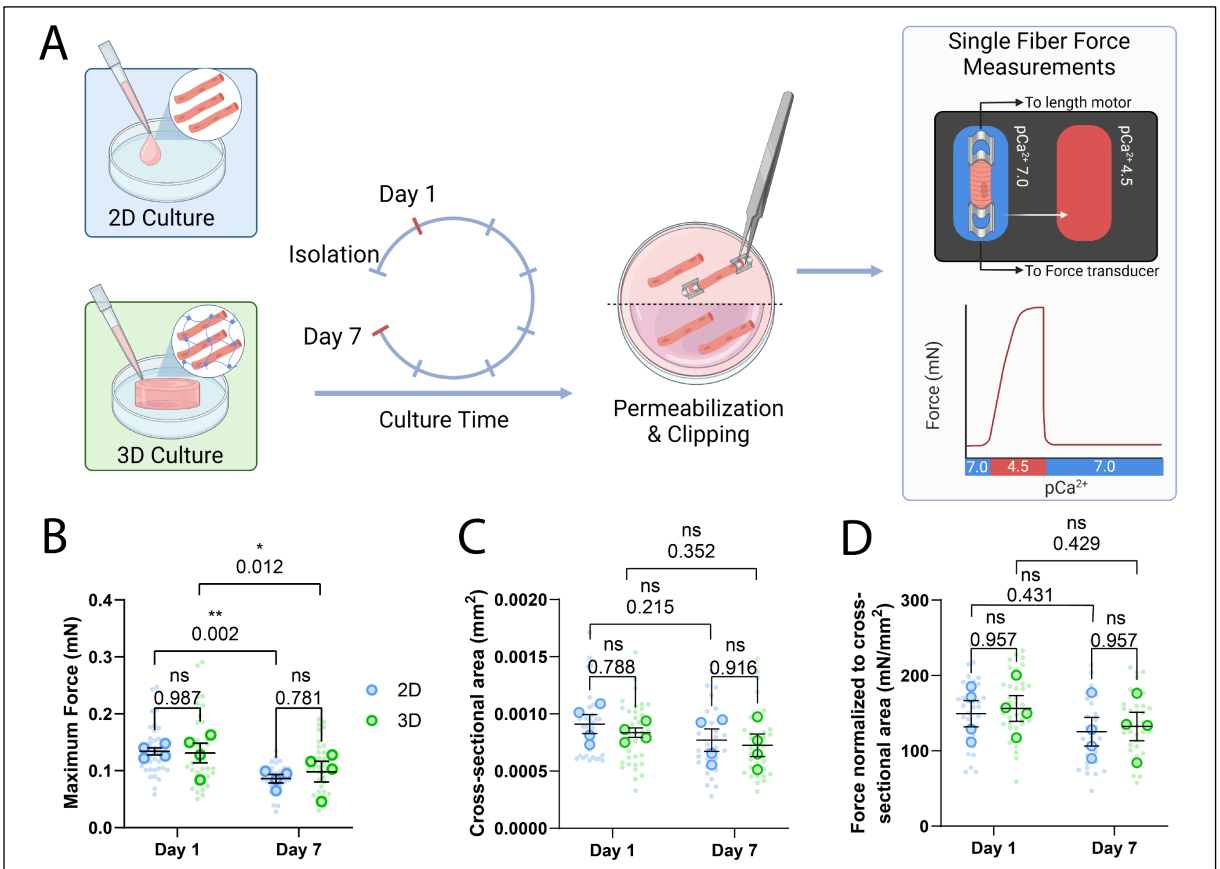

Figure 3: Single muscle fiber force measurements of muscle fibers cultured in 2D and 3D systems on Day 1 and Day 7 of culture. (A): Graphical overview of the force measurement experiment (Image made in Biorender®). (B): Quantification of the maximum force production of skinned muscle fibers at days 1 and 7 cultured in 2D and 3D. (C): Quantification of muscle fiber cross-sectional area at days 1 and 7 cultured in 2D and 3D. (D): Quantification of the normalized maximum force to cross-sectional area at days 1 and 7 cultured in 2D and 3D. Data are means ± SEM; N = 4 mice and n = fibers. Significance was determined using two-way ANOVA test with $p < 0.05$ considered as significant with * = $p < 0.05$ and ** = $p < 0.01$.

Reduction of contractile function in 2D is not caused by substrate adhesion

Since sarcomere organization and force production in muscle fibers cultured in 2D and 3D were conserved (**Fig. 3D**), the decrease in unloaded sarcomere shortening likely arises from a non-sarcomeric mechanism. Specifically, the discrepancy between preserved sarcomere organization (**Fig. 3**) and reduction in sarcomere shortening (**Fig. 2**) over time suggests that cells may become physically constrained over time. In addition, we observed that contractions of muscle fibers cultured in 2D were mainly impaired due to a reduction of sarcomere length at peak contraction (**Fig. S3**). Initially, we considered external constraints, since fibers cultured in 2D for 7 days showed sprouting of the fiber ends (**Fig. 2D**), which may be a sign of increased adherence to the substrate. Adherence to the relatively stiff tissue culture plastic could constrain muscle fibers, leading to shorter contractions. Therefore, we hypothesized that adhesion to the substrate may negatively influence contraction.

To investigate the role of adhesion in contractile function, we first aimed to determine whether adhesion complexes could recover in culture, since collagenase-based digestion is known to destroy extracellular sarcolemma proteins (Gineste et al., 2022). To assess the presence and recovery of adhesion complexes, we stained muscle fibers for α-dystroglycan to visualize the costamere complex on Day 1 and Day 7, in 2D and 3D (**Fig. 4A**). Our observations indicated that collagenase treatment disrupts this complex, which appears to be gradually reformed over the course of 7 days in both culture conditions. Although minimal protein recovery was noted on Day 1, muscle fiber membranes are completely covered in α-dystroglycan on Day 7. Between the fibers cultured in 2D and in 3D, no clear difference is visible in the costamere structure at Day 7. Thus, the expression of adhesion complexes does not appear to explain the difference in shortening between 2D and 3D culture conditions.

To directly explore the role of adhesion in muscle fiber function, we cultured muscle fibers in adherent (lamin-coated) or suspension conditions for 7 days. Additionally, a second 2D condition was included, in which muscle fibers were detached from the culture dish using trypsin at day 6 and replated to mimic conditions at Day 1 of culture (**Fig. 4B-D**). Across all tested conditions, no significant differences were observed in all measured contractile parameters. A slight downward trend is noticeable in the trypsin-treated fibers, likely due to harsh effects of trypsin on muscle fiber integrity. Trypsinization can increase cell membrane permeability (Dias and Nylandsted, 2021), potentially causing calcium leakage in the cells, which may in turn affect the sarcomere length in muscle fibers. Our measurements reveal that enzymatically dissociating muscle fibers disrupts adhesion complexes, which are reformed over the course of 7 days. Additionally, the absence or presence of adhesion complexes did not show any effect on the measured contractile parameters, suggesting that adhesion does not play a significant role in restricting contractile function in cultured muscle fibers, and consistent with our high-serum experiments that showed increased sprouting but no difference in sarcomere shortening (**Fig. S1**).

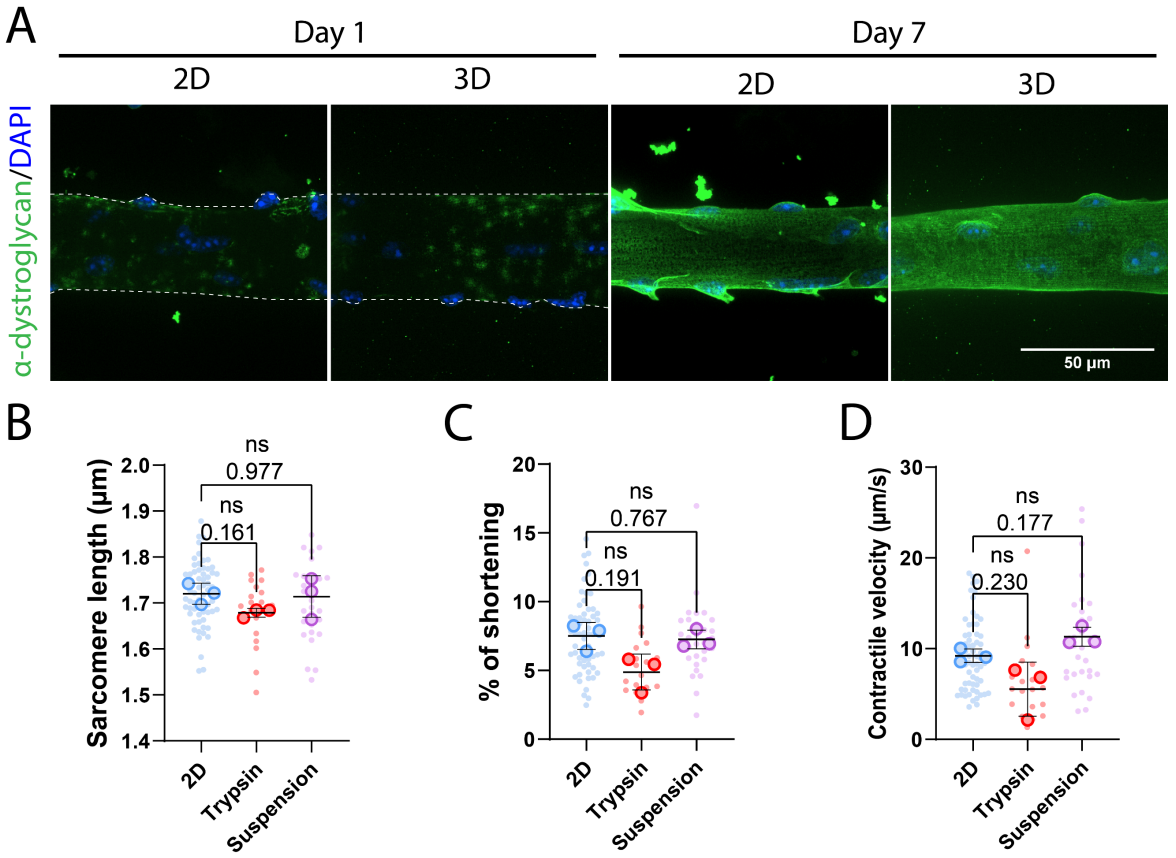

Figure 4: Influence of muscle fiber adhesion on contractility. (A): Representative confocal maximum intensity projection images taken with a 60x objective stained for showing a-dystroglycan (green) and nuclei (blue) in muscle fibers cultured for 1 and 7 days in 2D and 3D. Since treatment with collagenase destroys most membrane proteins, fibers are outlined with a dashed line at day 1. (B-D): Contractile measurements of muscle fibers cultured for 7 days in 2D, in 2D followed by dissociation with trypsin, or in suspension. (B): Quantification of resting sarcomere length of muscle fibers at day 7. (C): Quantification of the percentage of sarcomere shortening of muscle fibers at day 7. (D): Quantification of the contractile velocity of muscle fibers at day 7. Data are means ± SEM; N = 3 mice and n = fibers. Significance was determined using one-way ANOVA with $p < 0.05$ considered as significant.

Changes to microtubule organization impedes contractile function of skeletal muscle fibers following prolonged culture

Our previous data demonstrates that changes in fiber health and function in culture cannot be easily explained by changes in sarcomere organization/function or external constraints due to cell-substrate adhesion. Recent studies in cardiomyocytes have shown that non-sarcomeric cytoskeletal structures, such as microtubules (MT), can significantly influence contraction (Henderson et al., 2017, Robison et al., 2016, Caporizzo and Prosser, 2022). Building on previous results and the involvement of MT in cardiomyocyte contraction, we sought to investigate if MTs play a role in the loss of contractile performance in cultured muscle fibers, taking advantage of the fact that MT network can be readily manipulated with pharmacological agents, such as Taxol (MT stabilization) and Nocodazole (MT depolymerization). First, we treated muscle fibers with either Nocodazole, Taxol or vehicle (Control) at days 1 and 7. Fibers were fixed and microtubules stained to determine the effectiveness of the treatment (**Fig. 5A**). Control muscle fibers on day 1 showed an MT lattice structure typical of healthy muscle fibers, with longitudinal tubules running along the myofibrils, and transversal tubules running along the Z-discs (Belanto et al., 2016, Belanto et al., 2014). This lattice structure appears to be disorganized and denser after 7 days of culture (**Fig. 5A**). As expected, muscle fibers treated with Nocodazole showed almost complete depolymerization of the MT network, leaving only the nocodazole-resistant perinuclear stable microtubules intact (Denes et al., 2021) (**Fig. 5A**). Treatment with Taxol had varying effects on fibers at day 1 and day 7 of culture. On day 1, treatment seemed to cause disorganization of the MT network similar to control fibers at day 7. These changes were in line with our expectations since Taxol is known to stabilize MT through post-translational modification and generate longitudinally bundled microtubules (Mian et al., 2012). Nevertheless, treatment on day 7 seemed to partially restore a normal MT lattice structure, apart from the accumulation of MT around the nucleus. The same interventions were performed in 3D cultured fibers, which revealed similar alterations in the MT network as those cultured in 2D (results not shown).

Next, we investigated if changes in the MT networks affected muscle fiber contraction at Days 1 and 7, in both 2D and 3D conditions. At Day 1 post isolation, both Nocodazole and Taxol did not have a significant effect on the sarcomere length, shortening and velocity values of muscle fibers in 2D and in 3D culture (**Fig. 5B-D**). On Day 7, sarcomere length and contractile speed are also not altered by treatment with Nocodazole or Taxol (**Fig. 5E, G**). Interestingly, treatment with Nocodazole at Day 7 significantly increased muscle fiber shortening by 50% in 2D, from 5% to 7.5% (**Fig. 5F**). Taxol treatment shows a similar trend, but this change was not significant. In the 3D culture condition, both Nocodazole and Taxol treatment at Day 7 increased sarcomere shortening significantly, from ~7.5% to ~10%. These results indicate that changes in the microtubule network may contribute to a reduction in contractile function during prolonged muscle fiber culture, independent of whether cells are cultured in 2D or 3D. Strikingly, the combination of 3D culture and treatment with either Nocodazole or Taxol restored sarcomere shortening to a range found in muscle fibers on Day 1 (**Fig. 5F**). To summarize, we reveal that microtubule network changes over time independent of culture conditions. Furthermore, our contractile experiments revealed that changes to the MT network can significantly influence sarcomere contraction in cultured muscle fibers, providing evidence that the cytoskeletal network plays a prominent role in muscle fiber contraction.

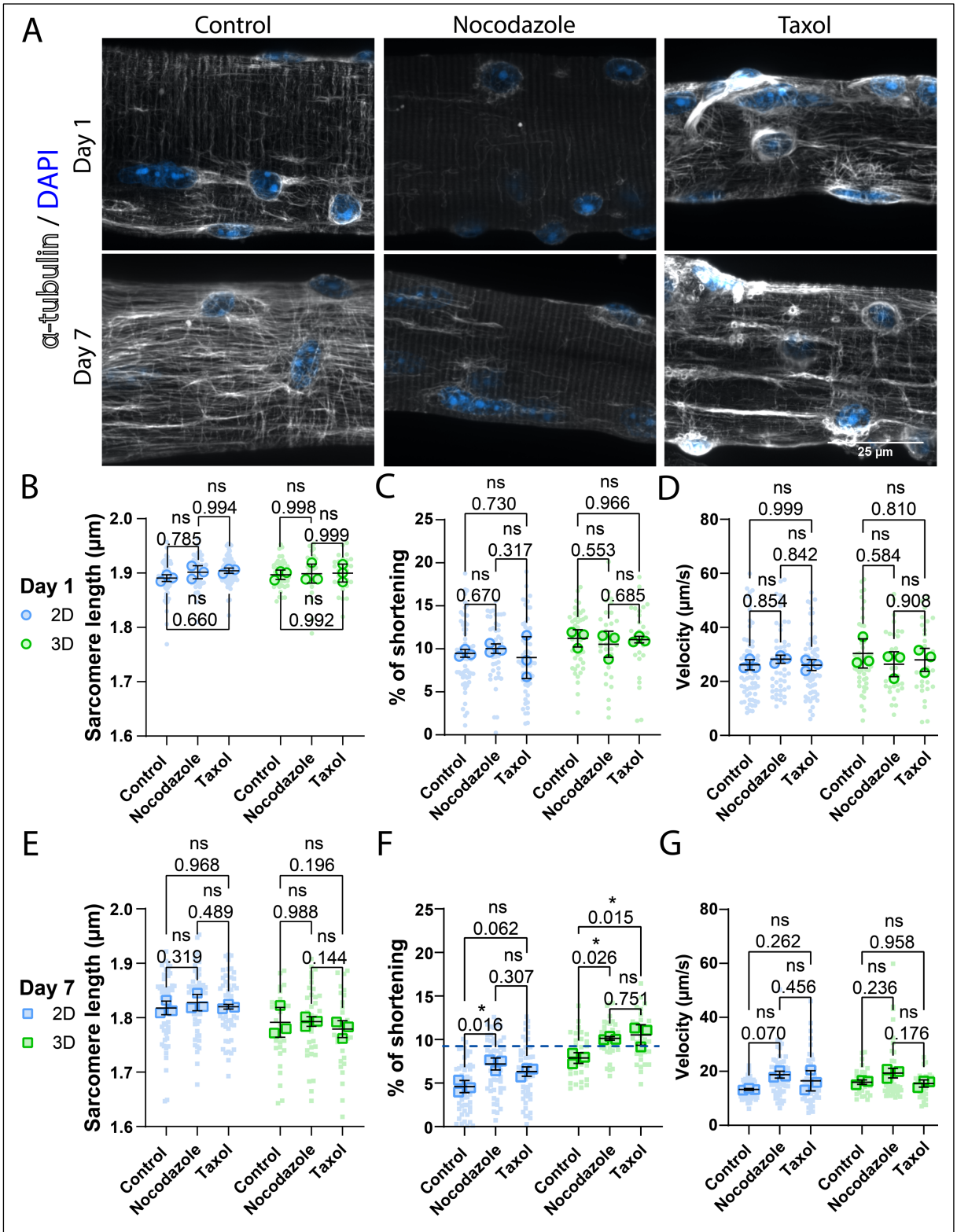

Figure 5: Microtubule networks in muscle fibers change during ex vivo long-term cultivation, thereby impairing sarcomere shortening. (A): Representative confocal maximum intensity projection images taken with a 60x objective stained for showing α-tubulin (grey) and nuclei (blue) in muscle fibers cultured for 1 and 7 days in 2D and 3D. (B-D): Quantification of contractile measurements of muscle fibers cultured in 2D and 3D at Day 1, treated with Nocodazole, Taxol or untreated (control). (E-G): Quantification of contractile measurements of muscle fibers cultured in 2D and 3D at Day 7, treated with Nocodazole, Taxol or untreated (control). Data are means ± SEM; $N = 3$ mice and n = fibers. Significance was determined using one-way ANOVA with $p < 0.05$ considered as significant with * = $p < 0.05$.

Discussion

In this study, we sought to gain a deeper understanding of culture-induced muscle fiber deterioration, as well as develop an improved culture system for *ex vivo* muscle fiber culture. To do this, we employed a recently developed optics-based, high-throughput contractile measurement system (Vonk et al., 2023). We first determined if contractile function decreases during culture at a similar rate as previously reported dedifferentiation of muscle fibers in culture (Renzini et al., 2018, Brown and Schneider, 2002, Rosenblatt et al., 1995, Keire et al., 2013, Duddy et al., 2011). In line with previous reports, muscle fibers kept in culture for 7 days on laminin-coated dishes undergo dedifferentiation and show signs of atrophy in both muscle fiber length and width (Keire et al., 2013, Duddy et al., 2011). Dedifferentiation of muscle fibers *in vitro* may be attributed to an innate response to muscle injury (Mu et al., 2011). This process is exacerbated by the addition of serum to the culture medium and might be caused by growth factors present in the serum. Adding onto these findings, we reveal that the culture of muscle fibers also causes a reduction in sarcomere length and contractile function. Muscle fiber atrophy is typically linked to both a reduction in the number of sarcomeres in series along the length of the muscle fibers, as well as a decrease in the fiber CSA (Adkins et al., 2021, Schiaffino, 2017, Hooper, 1981). Chronic muscle shortening, in particular, can lead to the loss of serial sarcomeres, contributing to muscle atrophy (Adkins et al., 2021, Schiaffino, 2017). In our long-term *ex vivo* culture setup, isolated muscle fibers remain unloaded and inactive for 7 days, resulting in a significantly lower sarcomere length than *in vivo* (Llewellyn et al., 2008). Therefore, the likelihood that our cells are subject to chronic shortening stress, and consequently the loss of serial sarcomeres, is rather high. Despite this, our measurements of muscle fiber length and sarcomere length revealed a similar percentile decline in both, indicating that the reduction in muscle fiber length is likely driven by the reduction in sarcomere length, rather than by a loss of sarcomeres. Using our long-term *ex vivo* culture setup, we use contractile function to assess the quality of cultured muscle fibers. Although contractile function can be used to assess fiber quality, we found that loss of function is not intrinsically linked to dedifferentiation. In line with other studies, muscle fibers treated with high serum medium underwent more dedifferentiation than those in low serum medium (Renzini et al., 2018, Brown and Schneider, 2002, Rosenblatt et al., 1995). However, other than resulting in a reduced resting sarcomere length, the induced dedifferentiation did not exhibit a clear decrease in contractile function compared to fibers kept in low serum conditions. These results suggest that the mechanism of dedifferentiation is not the main driver for functional reduction in cultured muscle fibers.

Since loss of function is not directly linked to dedifferentiation, it is unlikely that alterations in the culture media alone can ameliorate these effects. In their native environment, muscle fibers are continuously exposed to contraction-induced forces and mechanical cues from their extracellular environment (Zhang et al., 2021, Csapo et al., 2020). However, during the isolation procedure, muscle fibers are denervated and removed from their environment, leaving them unloaded and not exposed to any mechanical forces. Additionally, mature muscle fibers do not spontaneously contract (Pham and Puckett, 2024), meaning they do not experience the contractile forces necessary for normal muscle function (van Ingen and Kirby, 2021). Integrating contractile stimuli into an *ex vivo* culture system requires careful optimization of stimulation magnitude and frequency, which may change with culture duration. Thus, we opted to focus on the effect of mechanical cues from the extracellular environment, like substrate stiffness, which can be easily implemented in the *ex vivo* muscle culture platform as described in our previous work (Vonk et al., 2023). To test this, we embedded muscle fibers in a fibrin/basement membrane hydrogel to provide a scaffold with an anchoring surface. Our findings show that providing muscle fibers with a 3D environment increased viability of muscle fibers, while also preventing dedifferentiated morphology and sprouting of fibers. In the study performed by Brown and Schneider (2002), it was shown that embedding fibers in an agarose gel did not reduce the sprouting of muscle fibers ends in culture. Since agarose is a bio-inert gel and does not provide an anchoring surface, it seems that both the 3D structure and

attachment to the matrix are crucial in reducing this dedifferentiation. *In vivo*, muscles are physically connected to the bone via tendons, and to the ECM surrounding muscle fibers. These physical connections contribute to resistance, which partially provides the muscle with passive stretch and keeps sarcomeres at a working length of 3.15 - 2.55 µm (Ward et al., 2020, Llewellyn et al., 2008). Using our fibrin-based hydrogel, we provide muscle fibers with an extracellular structure in an attempt to reintroduce some of the structure lost during the enzymatic isolation procedure. The presence of this hydrogel may provide enough mechanical resistance to prevent hypercontraction and improve muscle fiber viability. Potentially, the sprouting observed in 2D culture conditions and reported in agarose gel may be an attempt for muscle fibers to reconnect muscle fiber ends to the tendon and regain this lost passive stretch. Functional measurements revealed that providing this environment also helps to maintain contractile function over time. Initially, we theorized that the addition of a matrix might help retain sarcomere lengths in culture, since the matrix may provide an attachment surface that prevents muscle shortening. Resting sarcomere lengths of fibers cultured in 3D decreased significantly compared to those cultured in 2D when measured using the Multicell system, but these findings were not reproduced when measuring sarcomere length in the same muscle fiber over time. It still not clear what caused this discrepancy, since sarcomere lengths were similar using both forms of measurements at Day 1. A deeper look into sarcomere shortening revealed fibers cultured in 3D maintain a higher shortening since they exhibit significantly shorter sarcomere length at peak contraction when compared to the 2D condition. As of yet, it is still unclear what drives these changes and how this impacts fiber integrity.

To further explore the factors that drive this observed decline in muscle fiber contractility, we opted to determine if changes in function were caused by direct changes in sarcomeric force generation. By measuring force generation of permeabilized fibers cultured in 2D and 3D at different time points, we were able to assess if the changes were caused by changes at the sarcomere level. These measurements revealed that while absolute force generation of muscle fibers decreased over time, no changes between 2D and 3D cultured fibers were apparent. A potential reason for the observed decay in absolute force could be the consequence of inactivity of muscle fibers for 7 days. CSA measurements also revealed no significant atrophy in any of the measured groups, although a similar trend was seen in previous measurements. This may have several causes, such as increased spread of data in this method or swelling of fibers due to permeabilization (Watanabe et al., 2019, Takemori et al., 2007). Nonetheless, when calculating the normalized force for each muscle fiber using these CSA measurements, no meaningful change in normalized force was observed in any of the groups. While a slight downward trend is seen, these results suggest that the contractile changes we see cannot be explained by a reduction of force generation of the sarcomeres, particularly the differences observed between muscle fibers cultured in 2D and 3D.

Since the changes we observed could not fully be explained by force generation or increased substrate adhesion, we decided to investigate the role of the MT cytoskeletal network in muscle fiber contraction. The involvement of MTs in sarcomere contraction has previously been demonstrated in cardiomyocytes (Robison et al., 2016, Caporizzo and Prosser, 2022) and muscle fibers (Kerr et al., 2015), where the MT network was shown to play a crucial role in contractile dynamics by buckling and bearing load during contraction. In line with this study, our data supports the importance of cytoskeletal network involvement in the contractile function of skeletal muscle fibers. Notably, immunofluorescent imaging revealed that the muscle fiber MT network is visibly altered during culture, and changes to the MT network at Day 7 using Taxol and Nocodazole were both able to influence sarcomere contraction. Since disruption of the MT network with Nocodazole improved contraction only at Day 7, we hypothesize that the observed alterations to the MT network on Day 7 can constrict sarcomeres, hindering their function. More interestingly, we found that Taxol was able to increase contractions of already constrained sarcomeres at Day 7, despite having no significant effect on Day 1, consistent with previous reports (Kerr et al., 2015). Taxol is known to increase posttranslational modifications (PTMs) of MTs, such as acetylation and detyrosination, which stabilize the MT network

(Weaver, 2014). In cardiomyocytes, an increase in MT detyrosination has been shown to increase coupling of MTs to sarcomeres, resulting in increased resistance and lowered contraction (Robison et al., 2016). Similarly, reducing MT detyrosination increases contractility in cardiomyocytes, and to a lesser extent skeletal muscle fibers (Kerr et al., 2015). In addition, increasing acetylated MT decreases contraction in cardiomyocytes and skeletal muscle fibers (Coleman et al., 2021). These results suggest that the improvement of contractile function we observe at Day 7 with Taxol treatment is unlikely due to its effects of increasing detyrosinated or acetylated MT, which would be predicted to further impair contractility. We hypothesize that long-term culture of muscle fibers may lead to detrimental organizational changes in the global organization or dynamics of the MT network, which can be alleviated with either nocodazole or Taxol treatment, leading to similar improvements in contractile function. Future studies should investigate the organization changes that occur in the microtubule network during prolonged culture, and whether these changes are driven by changes in the PTM profile, to better understand the mechanisms by which MT dynamics and/or organization influence sarcomere contraction and overall muscle function in this system.

One limitation of our study is that we were unable to measure intracellular calcium concentrations during contraction. Several changes in cultured muscle fiber contractile mechanics can be explained by changes in calcium handling by the muscle fibers. For example, changes in resting sarcomere length could be due to increased intracellular Ca^{2+}, while reductions in sarcomere shortening can be explained by reduced calcium release during contraction. Measurement of calcium transients proved to be technically challenging using the MultiCell system since it is optimized for cardiomyocytes instead of skeletal muscle fibers. Nevertheless, previous studies demonstrated that skeletal muscle fibers left in culture for up to 8 and 11 days, respectively, do not have altered Ca^{2+} levels both during rest and contraction (Brown and Schneider, 2002, Ravenscroft et al., 2007). Since these other studies report calcium handling does not change with long-term muscle fiber culture, it is unlikely that the decrease we see in contractile function after 7 days in culture is due to altered calcium transients. Nevertheless, we cannot rule out that changes in calcium handling are contributing to the increased contractile function in the 3D condition. Another limitation of this study is the complete inactivity and unloading of muscle fibers during culture. Inactivity, denervation and unloading are all known causes for muscle fiber disuse atrophy, which could explain some of our findings (Nunes et al., 2022). Since disuse of muscle may lead to reduced contractile function, further improvements to the culture system could focus on combining the 3D culture system with electrical stimulation during prolonged culture. Using such a method, muscle fibers would receive additional mechanical signals, reducing the effects of disuse on fiber function. Another possibility could be to introduce pneumatic stretch to the muscle fibers using flexible culture substrates. While such culture systems exist and show benefits in stem-cell derived cardiomyocytes (Kreutzer et al., 2020), passive stretch in muscle fibers should mostly be directed along the longitudinal direction of fibers, which is difficult to achieve in our culture system since muscle fibers are randomly aligned after the isolation procedure.

Long-term culture of explant muscle has long been a hurdle for *in vitro* skeletal muscle research. Since the first method of muscle fiber isolation was published in 1977 (Bekoff and Betz, 1977), several studies have looked into the effects of long-term culture of muscle fibers (Brown and Schneider, 2002, Ravenscroft et al., 2007, Pasut et al., 2013, Renzini et al., 2018, Rosenblatt et al., 1995). The results of these studies mainly illustrate the effects of serum in culture medium on muscle fiber morphology, revealing that proliferation medium with a high serum content drastically increases dedifferentiation of muscle fibers (Renzini et al., 2018, Brown and Schneider, 2002, Rosenblatt et al., 1995). By combining *ex vivo* culture with high-throughput contractile measurements, we revealed how *ex vivo* culture affects muscle fiber contractility and how these changes are associated with muscle fiber dedifferentiation. Changes to the culture system, such as embedding muscle fibers in 3D, illustrated how improving the system can diminish culture-induced functional deterioration. Further development of this 3D culture system, for example tuning matrix stiffness to a level similar to

in vivo muscle, may aid in maintaining muscle fiber contractile function *ex vivo*. Most strikingly, we revealed how microtubule structure changes over time, and how these structural alterations play a key role in modifying muscle fiber contractile dynamics. Collectively, our data highlights the importance of providing muscle fibers with a 3D environment during *ex vivo* culture, particularly when testing pharmacological or genetic interventions to influence viability or contractile function.

Acknowledgments and funding

We would like to thank Sanna Luijcx, Nienke ten Cate, and Eva Larose for their help with muscle fiber isolation and culture. We would like to thank Sylvia Bogaards for the scientific discussion on *ex vivo* culture conditions. Lastly, we would like to thank Michiel Helmes and Valentijn Jansen for their help and expertise in optimizing the Multicell setup and analysis. This work was funded by internal funding from the Department of Physiology (T.J.K) and a research grant from A Foundation Building Strength for Nemaline Myopathies and from Prinses Beatrix Spierfonds (W.OR23-06) (CACO).

Abbreviations

CSA	Cross sectional area
ECM	Extracellular matrix
FDB	Flexor digitorum brevis
MT	Microtubule

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