Multiplexed encoding of frequency-modulated sweep features in the inferior colliculus

Abbreviated title: Multiplexed encoding of FM sweep features in the IC

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Abstract

      Within the central auditory pathway, the inferior colliculus (IC) is a critical integration center for ascending sound information. While IC neurons have well-characterized receptive fields for individual sound features such as sound frequency, intensity, and location, growing evidence suggests that some neurons also use multiplexing to encode sound feature combinations. Here, we performed in vivo juxtacellular recordings in awake, head-fixed mice to examine how individual IC neurons and neuronal populations encode the speed, direction, and frequency range of frequency-modulated sweeps. To understand the strategies used by neurons to represent different sound features, we trained a support vector machine to decode sound features from different parameters of the spike train, including the firing rate, spike times relative to stimulus onset, distribution of inter-spike intervals, and first spike latency. We found that many IC neurons multiplex features of frequency-modulated (FM) sweeps using distinct temporal coding strategies rather than simple changes in mean firing rate, and that these feature representations are interdependent, yielding a combinatorial encoding of sound features within individual neurons. Accordingly, using static receptive fields for sweep frequency or direction alone yielded poor predictions of neuron responses to vocalizations that contain simple frequency changes. Lastly, we showed that encoding strategies varied across individual neurons, resulting in a highly informative population code for FM sweep parameters. Together, our results suggest that multiplexing is a common mechanism used by IC neurons to represent complex sound features.

Introduction

   One of the primary functions of the brain is to build representations of complex sensory objects based on the relatively limited set of features encoded by the sensory periphery. Many previous studies have shown that neurons in the inferior colliculus (IC), the midbrain hub of the central auditory pathway, are tuned to specific sound features. For example, IC neuron firing rate can be modulated by the frequency and intensity of pure tone stimuli (Suga, 1964; Ramachandran et al., 1999; Palmer et al., 2013), and IC neurons can exhibit firing-rate based tuning for sound duration (Casseday et al., 1994; Ehrlich et al., 1997; Fuzessery and Hall, 1999; Pérez-González et al., 2006) and sound location (Aitkin et al., 1984; Kuwada et al., 1987; Davis et al., 2003; Chase, 2005; Slee and Young, 2011). Prior studies also suggest that some IC neurons use changes in firing rate to encode the direction of rapid movements across sound frequency known as frequency-modulated (FM) sweeps (Suga, 1965; Poon et al., 1991; Fuzessery, 1994; Fuzessery et al., 2006; Andoni et al., 2007; Xie et al., 2007; Gittelman et al., 2009; Kuo and Wu, 2012; Geis and Borst, 2013).

   However, individual neurons have many available strategies by which they can encode sound features. In addition to firing rate, neurons can use the temporal patterning of spikes, including the timing of spikes over the duration of the stimulus, the inter-spike interval distributions, and/or first spike latency to transmit information about stimuli to postsynaptic partners. Neurons can also use combinations of these strategies to encode more than one stimulus feature in a single spike train, a coding approach called multiplexing. Evidence for multiplexing in auditory neurons has been found in auditory cortex (Furukawa and Middlebrooks, 2002; Lakatos et al., 2007; Walker et al., 2011; Insanally et al., 2019), and growing evidence suggests it also exists in IC (Zheng and Escabí, 2008; Day and Delgutte, 2016; Caruso et al., 2018). For example, the spiking patterns of single IC neurons carry information about three sound localization cues (Chase and Young, 2008), and IC neurons can also co-encode information about sound and task-relevant variables in a behavioral task (Quass et al., 2024). In addition, IC neurons can simultaneously encode information across sensory modalities, including visual and auditory stimuli (Schmehl et al., 2025).

Multiplexing sound features within single IC neurons requires the use of multiple coding

strategies. While most previous studies have focused on rate coding as the primary way that IC

neurons convey information about sound features, temporal codes also play a strong role in the

IC in the form of first-spike latencies (Chase and Young, 2008; Zheng and Escabí, 2008; Chot and

Zhang, 2025) and phase-locking to stimulus features (Joris et al., 2004; Nelson and Carney,

2007; Cai and Dent, 2020). Emerging evidence suggests that temporal codes are also important

in higher-order auditory structures such as auditory cortex (Bagur et al., 2025). This raises the

possibility that IC neurons could use combinations of changes in spike timing and spike rate to

multiplex features of complex sounds, but whether and how IC neurons use such coding

strategies is not well understood.

To examine this, we performed in vivo, juxtacellular recordings from IC neurons in awake

mice during presentations of frequency-modulated (FM) sweeps and used neural decoding to

examine how sweep features are encoded within spike trains. We found that FM sweep features

including sweep direction, speed, and frequency range could be decoded from the mean firing

rates, time-binned spike counts, ISI distributions, and/or first spike latencies in individual

neurons, revealing that IC neurons use many strategies to encode stimulus-specific information.

In addition, neuron responses to simple sound features such as sweep direction did not predict

responses to complex sounds such as vocalizations, indicating that complex sound responses

are not a simple extension of neuron tuning properties. Overall, these heterogeneous sound

responses in individual IC neurons yielded a population code that robustly represented complex

sound features. Thus, our results show that many IC neurons use multiplexed coding strategies

and that multiplexing at the individual neuron level can yield effective population codes for

complex auditory stimuli.

Results

IC neurons in awake mice use spike rate and timing to encode the direction of four-octave FM

sweeps

Many previous studies quantified direction selectivity for FM sweeps by determining the

sweep direction (up or down) that elicits a larger number of spikes (Fuzessery et al., 2006;

Gittelman et al., 2009; Kuo and Wu, 2012; Geis and Borst, 2013; Morrison et al., 2018), ignoring

the roles that spike timing might play in encoding information about sweep identity. To

overcome this problem, we performed in vivo juxtacellular recordings from IC neurons in awake,

head-fixed mice (**Figure 1A-B**) and examined direction encoding using both an asymmetry index

comparing the number of spikes elicited in each sweep direction and a machine learning model

that was trained on the time-binned spike counts for each trial. Recordings covered the

tonotopic map of the IC with neuron best frequencies (the frequency eliciting the greatest

number of spikes at 70 dB SPL) ranging from 4-64 kHz (**Figure 1C**). To investigate direction

selectivity, we played 70 dB SPL logarithmic FM sweeps with speeds of 10 – 200 octaves/second.

Neurons exhibited a diversity of responses, including direction selectivity (**Figure 1D-F**, first and

third cell), asymmetries in spike timing between up and down sweeps (**Figure 1D-F,** second cell),

and inhibition (**Figure 1D-F,** fourth cell). We first evaluated direction selectivity for neurons in

our dataset using the direction selectivity index (DSI), which is a normalized comparison of the

firing rates of the neuron during the up sweep compared to the down sweep (see equation in

Methods). Neurons with a DSI closer to +1 have higher firing rates in the upward sweep

direction, while neurons with a DSI closer to -1 have higher firing rates in the downward

direction (Kuo and Wu, 2012). We found that the DSIs of the cells we recorded from formed a

continuum (**Figure 1I**), with most cells being non-selective according to the criteria of Kuo and

Wu, 2012 (37/46 cells, defined as DSIs < +0.33 and > -0.33). Of the 9 cells that were directionally

selective according to the DSI metric, 4 were selective for downward sweeps and 5 were

selective for upward sweeps.

However, the DSI measure only considers the total number of spikes occurring during

the up or down sweep, disregarding information about spike timing that could be used by

downstream neurons to decode direction. To overcome this problem, we used a linear support

vector machine (SVM), a supervised machine learning approach that classifies data points by

fitting linear hyperplanes that separate classes (sweep directions) in a high-dimensional space.

We trained an SVM on the time-binned spike counts from up and down sweep trials to

investigate whether the direction of the sweep could be decoded from the spike trains of

individual IC neurons (**Figure 1G**, example shown uses 16 time bins principal components

analysis (PCA) transformed and projected onto the first two principal components for illustrative

purposes). Using the model, we found that the direction of the FM sweep could be determined

significantly above chance in 25/46 neurons (**Figure 1H**). Interestingly, we found that the group

of neurons where direction could be significantly decoded using the model did not completely

overlap with the group of neurons that were deemed directionally selective using the DSI.

Specifically, we found that sweep direction could be decoded from 20 cells that had non-

selective DSIs and we found no significant correlation (r^2 = 0.01) between the absolute value of

neuron DSI and model accuracy (**Figure 1J**).

We hypothesized that the mismatch between the DSI and model results occurred in part

because the timing of spikes, which is present within the time-binned spike counts and

accessible to the SVM but is not used by the DSI, contains information about sweep direction.

To test this hypothesis, we shuffled the order of the time bins within the time-binned spike

counts while maintaining class labels and compared the accuracy of the shuffled model to the

true accuracy (bin order intact) for each neuron. We found a significant decrease in the model

accuracy across all the cells when the time bins were shuffled (paired t-test, *t* = 7.0, *p* = 1.0e-8).

There were only 2 cells from which the direction could be decoded with shuffled bins compared

to 25 when the time bin order was intact, suggesting that the timing of spikes, rather than just

the total number of spikes, is critical for encoding direction in individual neurons (**Figure 1K**). In

particular, we found that cells that more accurately encoded direction had the largest shifts in

accuracy after the time bins were shuffled (**Figure 1K,L**), suggesting that cells that encode

direction well are more likely to use temporal codes. Overall, these results suggest that neurons

use a combination of strategies including both the timing of individual spikes and the overall

firing rate to encode sweep direction for FM sweeps.

Direction encoding for four-octave FM sweeps varies across sweep intensities but not speed

We next investigated how neural tuning for sweep direction is affected by changes in

sweep speed and sweep intensity. We hypothesized that sweep decoding would be highest at

slower sweep speeds, given this would exaggerate the asynchronies in activation of excitatory

and inhibitory areas of a neuron's tonal receptive field that have been suggested to underlie

sweep selectivity (Xie et al., 2007; Kuo and Wu, 2012). To examine this, we played upward and

downward four-octave FM sweeps with speeds varying from 10 – 200 octaves/second at four

different sound intensities (10, 30, 50, and 70 dB SPL, **Figure 2A**) and used an SVM to decode

the sweep direction at each intensity level and each speed. In line with our hypothesis, we

found that there was a significant difference in direction decoding across speeds (**Figure 2B,**

repeated-measures ANOVA, $F(9, 414) = 2.5$, $p = 0.0077$). However, post-hoc tests revealed that

none of the pairwise accuracies were significantly different from each other (Tukey's HSD, **Figure**

2C). In addition, while the number of cells from which direction could be decoded increased as

speed decreased, this trend was also not significant (Chi-square test for trend, $\chi^2 = 3,69$, $p =$

0.93). These results suggest that some IC neurons can robustly encode the direction of four-

octave FM sweeps across the tested range of sweep speeds.

Next, we tested whether direction decoding accuracy was also robust across FM sweeps

with varying intensities. We hypothesized that decoding accuracy would be highest at the

loudest intensity tested (70 dB SPL), as this would again exaggerate spiking differences between

inhibitory and excitatory areas in a neuron's receptive field and lead to greater asymmetries in

spike timing between up and down sweeps. In addition, IC neuron tonal receptive field shapes

exhibit intensity-dependent changes in frequency tuning (Palmer et al., 2013), suggesting that

direction selectivity may also be intensity-dependent. In line with this, we found that direction

decoding accuracy in IC neurons differed across varying sweep intensities within individual

neurons (**Figure 2D**, repeated-measures ANOVA, $F(3, 138) = 12.38$, $p < 0.0001$), with decoding

accuracy at 70 dB SPL significantly higher than decoding accuracy at 10 dB SPL (Tukey's HSD, $p =$

0.0001, **Figure 2E**). In addition, we observed that the number of cells from which direction could

be decoded increased as intensity increased (10 dB SPL: 5/46 cells, 30 dB SPL: 14/46 cells, 50 dB

SPL: 16/46 cells, 70 dB SPL: 27/46 cells), and this trend was significant (Chi-square test for trend,

$\chi^2 = 11.97$, $p = 0.007$).

Overall, our data show that direction decoding accuracy for four-octave FM sweeps is

relatively stable across sweep speed but not sweep intensity, with cells exhibiting higher

decoding accuracies at higher intensities.

Individual IC neurons robustly encode frequency range and speed but not direction of FM sweeps across varying sweep frequency ranges

Our results support the idea that some IC neurons encode sweep direction for four-octave FM sweeps. However, natural sounds rarely contain FM sweeps with such large frequency changes: many ethologically relevant sounds such as vocalizations have small frequency changes on the order of ½ to 1 octave (Holy and Guo, 2005; Portfors, 2007). Whether the direction of frequency change is encoded in IC neurons for smaller sweeps has been less well studied. To examine this, we presented both one- and two-octave FM sweeps at speeds of 10 – 200 octaves/second while recording from IC neurons in awake mice. One-octave FM sweeps consisted of the frequency ranges 4-8, 8-16, 16-32, and 32-64 kHz, and two-octave FM sweeps consisted of the frequency ranges 4-16, 8-32, and 16-64 kHz (**Figure 3A,B**).

To determine whether neurons were directionally selective, we used an SVM to decode the direction of the sweep from the time-binned spike counts of each neuron. Strikingly, we found that we could only decode direction from 2/31 of the cells in the one-octave sweep condition (**Figure 3C**, top), and in the two-octave condition, direction could only be decoded in 9/30 cells (**Figure 3D**, top). This finding differed from the four-octave sweep results, where direction was encoded in 25/46 cells, and suggests that selectivity for direction is not categorically encoded in individual mouse IC neurons for ethologically relevant FM sweep frequency changes.

Instead, we next asked whether other features of the sweep—in particular, the sweep frequency range and the sweep speed—could be decoded from each neuron's response. In contrast to the direction decoding results, we found that the speed of each sweep could be decoded significantly above chance from most cells in both the one- and two-octave sweep conditions regardless of sweep direction or frequency range (25/31 and 27/30 cells, respectively, **Figure 3C,D** middle). In addition, we found that the frequency range of the sweep, regardless of sweep direction or speed, could be decoded above chance in most cells in our dataset (31/31 cells for one-octave sweeps and 24/30 cells for two-octave sweeps, **Figure 3C,D** bottom).

Prediction errors made by the model varied for all three sweep features tested.

Decoding accuracy for the direction of one- and two-octave sweeps was near chance

performance, with the model predicting the sweep direction incorrectly almost as often as it

predicted direction correctly (**Figure 3E,F top**). Interestingly, for the one-octave sweeps the

model skewed towards predicting slower sweep speeds, with lower relative accuracy for fast

speeds (**Figure 3E, middle**), and the model tended to predict slower speeds than the actual

stimuli for most trials. This contrasted to prediction errors for the two-octave data, where the

model had highest accuracy in predicting both the fastest and the slowest sweep speeds, but

tended to predict the fastest speed even for trials that were slower (**Figure 3F, middle**). Sweep

frequency range decoding was similarly high across all sweep ranges tested (**Figure 3E,F**

bottom). Our data suggest that individual neurons do not categorically encode the direction of

one- and two-octave FM sweeps but instead provide information about other features of the

stimuli, such as the frequency range and speed.

Individual IC neurons multiplex features of FM sweeps

Previous literature suggests that individual IC neurons can jointly encode multiple sound

features. For example, IC neurons can multiplex information from multiple sound localization

cues with different features of a single spike train (Pena and Konishi, 2002; Chase and Young,

2008). IC neurons can also simultaneously encode visual and auditory information about a

sensory stimulus (Schmehl et al., 2025), and IC neurons show selectivity for both direction and

velocity for large FM sweeps (Andoni et al., 2007). We asked whether IC neurons that

significantly encode one sweep feature also significantly encode other features of a sweep by

correlating the decoding accuracies for direction, speed, and frequency range for each cell in

our one-octave (**Figure 4A**) and two-octave (**Figure 4B**) sweep data sets. We did not find a

significant positive correlation between direction and speed accuracies in the one- or two-

octave data (α corrected for 6 total comparisons using the Bonferroni correction = 0.0083;

linear regression, one octave: r^2 = 0.21, p = 0.019, two octave: r^2 = 0.20, p = 0.015). However,

direction and frequency range decoding accuracies were strongly correlated in both the one and

two octave datasets (one octave: r^2 = 0.65, p = 5.2e-8; two octave: r^2 = 0.69, p = 1.8e-8), as were

frequency range and speed decoding accuracies (one octave: r^2 = 0.40, p = 0.0001; two octave:

r^2 = 0.40, p = 0.0001).

These results suggest that many IC neurons can simultaneously encode multiple FM

sweep features, such as the frequency range and speed. Multiplexing features of an FM sweep

would require a neuron to use different strategies to represent different features within a single

spike train. There is previous evidence for multiplexing in auditory neurons: for example, in cat

IC (Chase and Young, 2008) and cat auditory cortex (Furukawa and Middlebrooks, 2002) sound

localization cues are encoded using multiple independent spike train features, including first

spike latencies and firing rate. Some evidence for multiplexing the features of large FM sweeps

also exists, with IC neurons showing selectivity for the direction and velocity of spectral motion

in bat (Andoni et al., 2007). However, the specific strategies used by IC neurons to multiplex FM

sweep features are not well understood.

One possibility is that in addition to overall firing rate, IC neurons use temporal

dimensions of their spike trains to encode sweep features. For example, the distribution of

inter-spike intervals (ISIs) can encode information in neurons independent of the temporal firing

rate patterns (Bialek et al., 1991; Panzeri et al., 2001; Lundstrom and Fairhall, 2006; Insanally et

al., 2019). The first spike latency (FSL) after stimulus onset can also carry important information

in auditory neurons, including in cochlear nucleus (Kitzes et al., 1978) and auditory cortex

(Phillips, 1988; Heil, 1997). We investigated which temporal strategies IC neurons use to encode

FM sweep features by training separate decoders to predict sweep direction, frequency range,

and speed from three different spike train representations: the time-binned spike counts (as

shown previously), the ISI distributions, or the FSL. Interestingly, decoding accuracy scores

obtained using each strategy were not significantly different from each other across the

population for decoding direction (Friedman test, one octave: $\chi^2(30)$ = 1.03, p = 0.60, **Figure 5A**,

two octave: $\chi^2(29)$ = 0.07, p = 0.97, **Figure 5G**), speed (one octave: $\chi^2(30)$ = 0.06, p = 0.96, **Figure**

5B, two octave: $\chi^2(29)$ = 2.87, p = 0.24, **Figure 5H**) or frequency range (one octave: $\chi^2(30)$ = 0.58,

p = 0.75, **Figure 5C**, two octave: $\chi^2(29)$ = 3.20, p = 0.20, **Figure 5I**).

However, it is possible that there is still diversity in coding strategies used by individual

neurons to encode different features—for example, some neurons may encode frequency range

using the time-binned spike counts while some may encode it using the ISI distribution. To

examine this, we correlated the decoding accuracies from each strategy in individual neurons.

Interestingly, in the one octave dataset we found that there was no correlation between

decoding strategies for sweep direction (r^2 = 0.002, p = 0.81, **Figure 5D**), speed (r^2 = 0.001, p =

0.86, **Figure 5E**), or frequency range (r^2 = 0.033, p = 0.33, **Figure 5F**). This suggests that neurons

tend to favor one strategy to encode a single sweep feature rather than redundantly encoding

the same information across both the time-binned spike counts and ISI distribution. In line with

this, we found neurons in our dataset that encoded information using the time-binned spike

counts and others that encoded information in the ISI distribution.

In contrast to results from the one-octave dataset, decoding accuracies from models

trained on the time-binned spike counts were correlated with models trained on the ISI

distribution in the two-octave dataset for direction (r^2 = 0.63, p = 1.4e-7, **Figure 5J**), speed (r^2 =

0.67, p = 3.4e-8, **Figure 5K**), and frequency range (r^2 = 0.77, p = 1.5e-10, **Figure 5L**). This

difference in decoding strategies for one- and two-octave data may suggest differences in how

neurons encode FM sweep information over time: given the shorter one-octave stimulus,

information about sweep features may be present in only one spike train metric, whereas the

longer two-octave stimulus may yield redundancy in coding strategies over the time course of

the sound. Overall, these data suggest that IC neurons multiplex information about FM sweeps

using different strategies that include the time-binned spike counts, ISI distribution, and first

spike latency.

Spike timing is important for encoding sweep speed but not sweep frequency for one- and

two-octave FM sweeps

We showed above that IC neurons encode sweep direction for four-octave sweeps in a

timing-dependent manner, such that disrupting the temporal information contained in the

spiking pattern while leaving the overall number of spikes intact significantly decreased the

direction decoding accuracy (**Figure 1K,L**). In addition, training the SVM on neuron time-binned

spike counts provided the highest accuracy in decoding the frequency range and speed of the

sweep in most neurons in the one- and two-octave datasets (**Figure 5**), suggesting that IC

neurons may also use spike timing to encode information about these features. To directly test

whether the timing of the spikes is critical for encoding these features, we trained separate

SVMs to classify sound features from the time-binned spike counts for one- and two-octave FM

sweeps. We then compared performance of the decoder with the time bins intact vs. with the

time bins for each trial in a shuffled order, which disrupted the temporal information in each

trial while preserving the total number of spikes.

We found that shuffling the order of the time bins in the one-octave condition

significantly decreased the accuracy of the model for sweep direction (**Figure 6A**, paired t-test, t

= 3.93, p = 0.0005), speed (**Figure 6B**, t = 4.61, p = 7.0e-5), and frequency range (**Figure 6C**, t =

5.62, p = 4.04e-6). In line with this, there were also fewer cells from which direction and speed

could be significantly decoded when the time bins were shuffled (direction: 0 shuffled vs. 2

unshuffled, speed: 13 shuffled vs. 25 unshuffled), but the number of cells that encoded

frequency range significantly above chance changed only minimally when the bins were shuffled

(29 shuffled vs. 31 unshuffled), even though mean decoding accuracy decreased. We found a

similar result in the two-octave condition, where shuffling the order of the time bins also

significantly decreased the accuracy of the model for direction (**Figure 6D**, t = 5.19, p = 1.51e-5),

speed (**Figure 6E**, t = 6.59, p = 3.22e-7), and frequency range (**Figure 6F**, t = 5.46, p = 7.08e-6).

Again, the number of cells that encoded speed and direction above chance decreased in the

shuffled condition (direction: 1 shuffled vs. 9 unshuffled, speed: 11 shuffled vs. 27 unshuffled).

However, despite a decrease in accuracy in the shuffled condition, the number of cells that

encoded frequency range above chance remained the same in both conditions (24 shuffled vs.

24 unshuffled).

These results suggest that spike timing may be more important for conveying sweep

speed compared to sweep frequency range, as frequency range decoding accuracy was less

affected by disruptions in spike timing. These findings further support the idea that IC neurons

can use different strategies to encode different sound features.

IC neurons encode sound features across multiple time scales

In the analyses above, decoding algorithms were trained on all the spiking information

from a neuron across an individual trial, such as the time-binned spike counts or distribution of

inter-spike intervals across hundreds of milliseconds. However, postsynaptic targets are

constrained in their ability to integrate inputs across time by the passive and active membrane

properties of the target neurons. While this could be seen a coding limitation, this constraint

would allow presynaptic neurons to encode different sound features at different times during

the response, which could then be read out by one or multiple postsynaptic neurons with

varying temporal integration windows.

To investigate this question, we trained an SVM to decode the direction, speed, and

frequency range of an FM sweep using consecutive 6.9 ms windows (3 combined time bins) of

each neuron's response to one-octave FM sweeps of varying directions, speeds, and frequency

ranges. We found that direction decoding was relatively poor throughout the duration of the

sound but peaked at the beginning of the stimulus (**Figure 7A**), an effect likely due to strong

onset spiking for one sweep direction in some cells. Decoding accuracy for sweep speed

occurred later compared to stimulus onset but remained high throughout the duration of the

sound (**Figure 7B**), whereas frequency range decoding increased rapidly after the onset of

sound and then decayed (**Figure 7C**, compared in **Figure 7D**). Direction decoding was better for

the two-octave sweeps compared to the one-octave sweeps and peaked at the stimulus onset

(**Figure 7E**). Decoding across time was similar for the other features of the two-octave FM

sweeps, with consistent decoding of speed throughout the duration of the stimulus (**Figure 7F**)

and a fast increase in decoding accuracy for frequency range (**Figure 7G**) at the beginning of the

stimulus.

We next asked how the accuracy for encoding each feature differed in time compared to

chance level. To do this, we normalized each accuracy score to the baseline pre-stimulus

accuracy (at chance level) and compared decoding accuracy over time for each feature. For both

one- and two-octave sweeps, we found that accuracy for frequency range increased first and

then declined, while speed decoding increased later than frequency range but was consistent

throughout the duration of the stimulus (**Figure 7D,H,** pink and purple lines). Relative to chance,

decoding accuracy for direction was poor across all time bins compared to the accuracy values

achieved for frequency range and speed (**Figure 7D,H** blue lines).

These results suggest that individual IC neurons can represent sound features across

varying time scales, which could provide another mechanism for downstream cells to receive

information about complex stimuli.

Populations of IC neurons provide robust representations of FM sweep features

While we found that decoding sweep frequency range and speed from individual

neurons was above chance in many cells, accuracy values were rarely high enough to provide

high-confidence information about the stimulus (**Figure 3**). However, the response

heterogeneity and multiple coding strategies used by individual IC neurons could comprise a

population code for various sound features. Population representations of other sound features,

including sound location and amplitude-modulated stimuli, have been previously shown in IC

neurons (Zohar et al., 2013; Day and Delgutte, 2016; Rogalla et al., 2024; Shi et al., 2024), but

population codes for FM sweep features have not been investigated. We examined the

population benefit for encoding the speed, frequency range, and direction of one- and two-

octave FM sweeps by grouping cells into pseudo-populations that consisted of 2-21 neurons and

compared the decoding accuracy for these groups to the accuracy obtained from single

neurons.

In the one-octave dataset, we found that increasing the number of neurons in the

pseudo-population (starting with decoding from individual cells) significantly increased the

decoding accuracy for direction (**Figure 8A**, $F_{(20,630)} = 58.85$, $p < 0.0001$), speed (**Figure 8B**

repeated measures ANOVA, $F_{(20,630)} = 141.8$, $p < 0.0001$), and frequency range (**Figure 8C,**

$F_{(20,630)} = 263.64$, $p < 0.0001$). As cells were added to the population, direction decoding

accuracy reached an asymptote that approached 65% accuracy when the population contained

approximately 15 cells (**Figure 8A**). Speed decoding accuracy increased nearly linearly with each

cell added to the population, and decoding accuracy was limited by the number of neurons in

our dataset and thus the number of cells that could be added to the population (**Figure 8B**).

Strikingly, frequency range decoding approached 100% accuracy and did not significantly

increase after the pseudo-population contained 16 cells, suggesting this population size could

reliably convey frequency range information for one-octave FM sweeps (**Figure 8C**).

Population decoding accuracies from the two-octave datasets largely mirrored those

from the one-octave results. Increasing the number of cells in the pseudo-population

significantly increased the decoding accuracy for direction (**Figure 8D**, $F(20, 609) = 137.74$, $p <$

0.0001), speed (**Figure 8E**, $F(20, 609) = 452.70$, $p < 0.0001$), and frequency range (**Figure 8F**,

$F(20, 609) = 290.97$, $p < 0.0001$). Again, direction decoding accuracy was better in the two-

octave dataset compared to the one-octave dataset, and decoding accuracy began to plateau

around 15 cells at a decoding accuracy of 80% (**Figure 8D**). Speed decoding accuracy increased

with the number of neurons in our dataset, and the trend in the data suggests that increasing

the pseudo-population size would have continued to increase decoding accuracy (**Figure 8E**). In

addition, frequency range decoding again approached 100% at a pseudo-population size of

approximately 16 neurons (**Figure 8F**).

Overall, these results show that population codes convey more accurate information

about the features of FM sweeps than individual IC neurons.

Frequency change direction for vocalizations is not encoded in individual IC neurons

Both human speech and mouse vocalizations contain rapid frequency sweeps (Portfors,

2007), and previous studies have shown that some IC neurons fire selectively for specific

vocalizations (Portfors et al., 2009; Mayko et al., 2012; Lawlor et al., 2025). However, whether

the frequency sweeps present in conspecific vocalizations shape individual neuron selectivity is

not well understood. To examine this, we recorded from IC neurons while playing four types of

calls (calls from Schiavo et al., 2020; Valtcheva et al., 2023): an ultrasonic upsweep, an ultrasonic

downsweep, an ultrasonic vocalization with complex (up and down) frequency changes, and a

call with multiple low-frequency bands (in order, we refer to these as upsweep, downsweep,

complex, and wriggle, **Figure 9A**).

Consistent with previous studies, we found that some neurons exhibited selective

responses for specific vocalization classes. To quantify how well individual neurons encoded

vocalization class, we trained an SVM on the spike trains of individual neurons. The SVM

predicted the vocalization class above chance (25%) in 17/33 cells (**Figure 9B**), with an average

accuracy of 44% in cells with significant encoding. To investigate whether the direction of the

FM sweep within the vocalization was important for vocalization discriminability, we next

performed decoding on two sets of responses. For the first model, we grouped responses for

vocalizations where there was a true upsweep (upsweeps, and downsweeps played backwards)

and trained the decoder to discriminate these from responses where there was a true

downsweep (downsweeps, and upsweeps played backwards). Interestingly, we found that in

only 3/33 cells in our dataset could the direction of the vocalization be decoded significantly

above chance (**Figure 9C**), and average accuracy for cells with significant decoding was 62%,

suggesting that most IC neurons do not specifically encode the direction of frequency sweeps

contained within vocalizations.

We next asked whether the upsweep or downsweep vocalization class could be decoded

using the neuron time-binned spike counts regardless of whether the vocalization was played

forwards or backwards. Here, we found that 7/33 neurons could discriminate the class of the

sweep, and these neurons had higher accuracy (72%) compared to the decoding for the true

direction (**Figure 9D**). We examined the peri-stimulus time histograms (PSTHs) for the upsweep

and downsweep vocalizations in the neuron with the strongest decoding accuracy and found

exclusive responses to the downsweep vocalization regardless of what direction it was played

(**Figure 9E**), indicating that information other than the direction of the frequency change is

important for vocalization class selectivity in this neuron. In addition, we found that in this

highly selective neuron, the tonal receptive field overlapped with the frequency content of the

preferred vocalization (**Figure 9F**). However, this was not always the case: we obtained

frequency response areas (FRAs) from 6/7 neurons where vocalization class (up/down) could be

decoded significantly above chance and found that only two of them exhibited clear V-shaped

tuning. In one of these cells (240709_574), the preferred frequency was around 10 kHz, which

was much lower than the frequencies present in either vocalization (**Figure 9G**). The FRAs from

the remaining four neurons exhibited some tuning at higher intensities, but again tuning did not

overlap with the vocalization spectral content. These results indicate that vocalization selectivity

in the mouse IC cannot be readily extrapolated from simple tonal or directional receptive fields.

Discussion

Here, we used machine learning models to examine how multiple sound features of an

FM sweep, including the frequency range, speed, and direction, are encoded in the spike trains

of individual IC neurons. We found that single IC neurons can multiplex FM sweep features by

encoding information along multiple dimensions of the spike train, including the time-binned

spike counts, mean firing rate, ISI distribution, and first spike latency. In addition, we showed

that IC neurons can encode sound features at different time points during a stimulus, providing

an additional mechanism for multiplexing. We also examined decoding in pseudo-populations of

IC neurons and found that, when combined, the heterogeneous responses of single neurons can

yield robust population encoding of FM sweep sound features. Lastly, we showed that the

directionality of frequency sweeps has little influence on vocalization selectivity in single IC

neurons, indicating that complex sound responses may not be well-predicted by the receptive

fields generated in individual neurons for simple sound features.

Machine learning methods capture alternative coding strategies used by IC neurons

Many previous studies in the IC have investigated neuron selectivity for FM sweep

features using selectivity indices such as the DSI, a normalized measure that compares the total

number of spikes elicited by an up sweep to those elicited by a down sweep (e.g., Andoni et al.,

2007; Williams and Fuzessery, 2010; Kuo and Wu, 2012; Geis and Borst, 2013). Tonal receptive

fields that describe frequency selectivity in individual IC neurons are also typically constructed

by comparing the total number of spikes elicited by different sound frequencies. However, total

spike counts are only one way that neurons may encode sound features, and as sounds often

have rich temporal structures, evaluating selectivity using only summed spike counts may omit

temporal and other cues that could contain stimulus-encoding information. Indeed, emerging

evidence suggests that temporal coding strategies are important not just at early auditory

processing centers such as the cochlear nucleus, but also within higher-order auditory

processing centers including auditory cortex (Bagur et al., 2025). Evaluating neuron encoding

using only changes in spike rate also assumes that downstream neurons are acting only as

simple linear summators, but a plethora of electrophysiological evidence and computational

modeling suggests that this is not the case. For example, dendrites alone have numerous

mechanisms that support non-linear integration (Tamás et al., 2002; Gómez González et al.,

2011; see Palmer, 2014 for a review).

Here, we instead used an SVM to predict sound features from the neuron time-binned

spike counts, giving the model access to firing rate across time. We found that the direction of

four-octave FM sweeps could be decoded from the time-binned spike counts of many more cells

than would be predicted from the DSI. In addition, we showed that disrupting spike timing while

maintaining the firing rate for each trial significantly reduced the model decoding accuracy for

direction in four-octave sweeps. It also significantly reduced the decoding accuracy for direction,

sweep speed, and frequency range in one- and two-octave sweeps. These results indicate that

there is information conveyed in spike timing about not only the direction of FM sweeps but

also other sweep features, and this information is lost using methods that disregard spike

timing.

IC neurons multiplex sound features using several strategies

In this study, we highlight several temporal strategies that IC neurons use to encode

features of FM sweeps, including the time-binned spike counts, the ISI distribution, and the first-

spike latency (**Figure 5**). Previous studies in auditory cortex suggest that individual neurons can

use some of these strategies independently of each other (Insanally et al., 2019), providing a

mechanism by which neurons can multiplex features of sounds. Similarly, we found that IC

neurons multiplex features of FM sweeps, including the frequency range and speed (**Figure 4**).

These data are supported by other studies demonstrating joint encoding in IC neurons, for

example, with encoding of sound localization cues (Chase and Young, 2008), mixed

representations of sound and task variables during a behavioral task (Quass et al., 2024), and

dual encoding of auditory and visual stimuli (Schmehl et al., 2025). Ultimately, a critical step

toward understanding how IC neurons encode information will be to compare the encoding

strategies used in the IC and the decoding strategies used by postsynaptic targets, especially in

the medial geniculate body (MGB), the primary ascending target of the IC. To date, there have

been few studies investigating how MGB neurons decode information from the IC, and this is an

area of future research that is critical for understanding how sound information is represented

along the ascending auditory pathway.

IC neuron responses to complex stimuli are not simple summations of selectivity profiles

A common approach in past studies of the IC has been to categorize IC neuron responses

by their selectivity for (or tuning to) specific sound features. However, emerging evidence from

analyses of large neural datasets suggests that neuron responses are rarely truly categorical

(Raposo et al., 2014; Posani et al., 2024). Here, we found that individual IC neuron responses to

sweep direction varied with sweep speed and intensity (**Figure 2**). Such context-dependent

selectivity has been previously shown for sound and task-dependent variables in some IC

neurons (Quass et al., 2024) and for features of FM sweeps (Andoni et al., 2007; Andoni and

Pollak, 2011). In this study, we also found that even in neurons that encoded FM sweep

direction, this alone did not inform how those neurons responded to a vocalization with similar

directional changes (**Figure 9**). However, neuron selectivity for specific sound features may not

be necessary for and might even hinder robust population codes for stimuli within the IC. For

example, in neocortex, a recent study suggests that categorical responses typically underlie low-

dimensional rather than high-dimensional population responses (Posani et al., 2024). Similarly,

studies in the IC suggest that neuron population codes for amplitude-modulated stimuli do not

depend on neurons with high selectivity (Shi et al., 2024), and correlations generated between

categorical neurons constrain rather than enhance the amount of information that can be

contained in IC neuron populations (Zohar et al., 2013). Along the ascending auditory pathway,

there is also a clear decorrelation of neuron responses to simple sound features spanning from

IC to auditory cortex, suggesting that decreases in neuron selectivity parallel an increase in the

specificity of the population neural code for complex auditory objects (Gosselin et al., 2025). In

line with this, we found that the decoding accuracies from single neurons for sound features

was on average quite low (**Figure 3**), and we did not find evidence for cells that encoded

direction robustly across differing frequency ranges and speeds. However, pseudo-population

decoding accuracy was high (**Figure 8**) and increased with increasing neuron numbers in the

pseudo-population, pointing to robust population codes for FM sweep features in the IC that

are not constrained by a lack of selectivity for features within individual IC neurons.

Overall, our data suggest that individual IC neurons can multiplex sound features using

multiple strategies including both temporal and spike rate-based cues. However, most neurons

do not exhibit strong spike rate-based selectivity for features of complex sounds, and neuron

responses to sound features in a simple stimulus (e.g., sweep direction) do not entirely predict

how the neuron will respond to natural sounds that share similar characteristics (e.g., an

upward frequency sweep.) These data support an increased complexity in how neuron

responses to sound features are constructed along the central auditory pathway and provide a

powerful framework for understanding neural coding in the IC. An important next step for

future studies is to determine how the MGB and other brain regions that receive input from the

IC use the representation of complex sound features that arises from multiplexing in IC neurons.

Materials and Methods

Animals

All experiments were approved by the University of Michigan Institutional Animal Care and Use Committee and were in accordance with NIH guidelines for the care and use of laboratory animals. Animals were given continuous access to food and water and stayed on a 12-hour day/night cycle. Mice of both sexes were used, and all mice were on a CBA/CaJ or CBA/CaJ x C57BL/6J background to avoid the early-onset, age-related hearing loss caused by the recessive $Cdh23^{Ahl/+}$ mutation in C57BL/6J mice (Noben-Trauth et al., 2003). To further ensure that mice used did not exhibit hearing loss, mice were aged P61-P86 at the time of experiments, as mice on CBA/CaJ and CBA/CaJ x C57BL/6J backgrounds at this age range do not exhibit age-related hearing loss on auditory brainstem response tests (Kane et al., 2012). Additionally, during electrophysiological recordings, we evaluated neural thresholds for 200 ms pure tones over a frequency range of 4 to 64 kHz. All neurons that exhibited V-shaped frequency tuning curves had thresholds at 10 dB SPL, the lowest sound level tested.

Headbar implantation

Mice were anesthetized using 1-3% isoflurane (Piramal Critical Care, # NDC 66794-017-25), and body temperature was maintained using a homeothermic heating pad placed under the mouse. To reduce post-operative pain, mice were given subcutaneous injections of carprofen (5 mg/kg, CarproJect, Henry Schein Animal Health) and buprenorphine (0.1 mg/kg). Hair on the scalp was removed using scissors, and a circular portion of scalp approximately 11-12 mm in diameter was removed to expose the skull. The IC was identified using stereotaxic coordinates (relative to lambda and in µm: 900 caudal, 1125 lateral) and marked using a surgical marker. Bupivacaine (0.2 mL) was then applied to numb the skull, the periosteum was removed, and the skull was thoroughly scored using a #11 scalpel. To begin adhesive preparation for the headbar, a thin layer of dental acrylic (C&B Metabond from Parkell, cat #s S398, S399, S371) was applied using a fine paintbrush, which was then left to cure for ten minutes. On top, a thin layer of dental acrylic resin (Henry Schein, Inc., # 1259208 and # 1250143) was applied. Dental acrylic resin was also applied to a custom-designed headbar that was then placed onto the skull. To

secure the headbar to the skull, dental acrylic resin was added in layers to cover the top of the

headbar, and then silicone elastomer (Smooth-On Inc. Body Double FAST) was placed in the

opening over the skull and secured with a thin strip of dental acrylic resin. Mice were monitored

for signs of pain or distress for one hour post-procedure and were ambulatory before being

returned to the vivarium. An additional injection of carprofen was administered the day

following surgery for postoperative analgesia, and animals continued to be monitored for signs

of pain or distress for 7 days.

Craniotomy surgery

On the first day of recording, mice were anesthetized using 1-3% isoflurane. Body

temperature was maintained using a homeothermic heating pad placed under the mouse. To

reduce post-operative pain, mice were given a subcutaneous injection of carprofen (5 mg/kg,

CarproJect). Using the IC mark that was made during the headbar implantation procedure, a

craniotomy was made using intervals of drilling with a micromotor drill (K.1050, Foredom

Electric Co.) with a 0.5 mm burr (Fine Science Tools). Drilling began with shallow and small

circles and was interrupted every ~20 seconds with application of cold PBS to ensure brain

temperature was unaffected. When the skull above the IC was thin enough, a #11 scalpel and/or

27-gauge needle was used to remove a small section of skull above the IC. For one hour post-

procedure, mice were monitored for signals of pain or distress.

In vivo electrophysiology recordings

29 mice (14 female, 15 male) aged P61-P86 at the time of first recording were used for

the study. Mice began habituation to the head fixation setup 3 or more days following headbar

implantation to allow for recovery. Habituation consisted of one day of handling within the

mouse's cage and 3-5 days of head fixation inside the sound isolation booth, with the duration

of head fixation increasing every day until the mouse tolerated 80 minutes of head fixation. A

craniotomy was then surgically drilled above the left IC using the procedures outlined above

under "Craniotomy surgery". After one hour of recovery, mice were placed in the head fixation

setup on a floating air table. The recording pipette was backfilled with an in vivo internal

solution (in mM, 135 NaCl, 5.4 KCl, 1.5 CaCl$_2$, 1 MgCl$_2$, 5 HEPES, pH set to 7.3 with NaOH). The

recording was grounded to a silver chloride wire placed into a well of PBS surrounding the

craniotomy on the mouse skull. An MP-285 micromanipulator (Sutter Instrument) was used to

slowly advance the pipette into the IC, and neurons were identified for juxtacellular patch-

clamp recordings by an increase in electrode resistance and the presence of action potentials.

Once a loose seal was made with a cell (6-47 MΩ), a regularly calibrated, free-field electrostatic

speaker (Tucker-Davis Technologies, ES1) was used to present sound stimuli to the mice. The

speaker was positioned contralateral to the IC recording site, at ~10 cm in front of the right ear,

at a 45° angle. Sound stimuli consisted of logarithmic FM sweeps of varying sweeps, speeds,

intensities, and octaves (see Table 1), 100 ms white noise bursts (4-64 kHz, 70 dB SPL), and

various mouse vocalizations presented forwards and backwards. All stimuli except vocalizations

were generated in MATLAB, sampled at 192 kHz, and amplified using a TDT SA2 stereo amplifier.

Vocalizations were also sampled at 192 kHz and amplified using a TDT SA2 stereo amplifier. Data

were acquired at 50 kHz and low-pass filtered at 10 kHz using a Dagan BVC-700A amplifier, an NI

PCIe-6343 data acquisition board, and the WaveSurfer (Janelia) package in MATLAB

(Mathworks, 2022a-2024a). Individual mice were recorded from once daily for fewer than 10

sessions total. Recording locations were verified to be within the IC through post-hoc histology

to visualize the electrode penetration tract, which was evident due to tissue damage and/or

labeling with the fluorescent marker DiI (ThermoFisher Scientific, #V22885).

Analysis of electrophysiological recordings

Data were re-associated with stimuli information and metadata post-collection using a

custom MATLAB script. Spikes were detected using a threshold crossing approach. Detected

spikes were visually examined to remove any instances where motion or other artifacts were

incorrectly detected as spikes. Spike detection was further validated by performing k-means

clustering on the amplitude and full-width at half-maximum amplitude of each spike; recordings

that exhibited multiple clusters using this analysis were very rare and were excluded from the

dataset when they were found.

Machine learning models

Analyses were performed in Python 3.11.9. After data pre-processing (outlined above),

electrophysiology data were saved into a structure and imported to Python. Support vector

machine (SVM) models were implemented in Python using the 'SVC' function with a linear

kernel from the 'sklearn' package. When classification was performed on more than two groups,

a 'one versus rest' strategy was used. The C parameter was set to 1 for all models. The model

features were the time-binned spike counts from each trial, and the number of bins was

determined by examining model performance across 1-501 bins (steps of 2) for decoding

direction of the FM sweep. The resulting bin sizes are shown in Table 2. To maintain consistency

across each model, we used the bin size that resulted in the highest accuracy (2.3 ms) as

features for each model. The resulting number of bins for each stimulus is shown in Table 2. The

total time binned for each stimulus corresponded to the longest duration FM sweep for that

stimulus set plus 20% of the stimulus time to account for time delay for sound to reach the IC

and any offset spiking that might contribute to coding.

After binning, models were trained on 80% of the data and tested on 20% of the data

using 5-fold cross validation. In cases where direct comparisons were made between the sound

feature decoding accuracy scores in the same neuron (for different sound features), the data

were downsampled to the sound feature with the lowest number of observations and the

average k-fold cross validated accuracy from each of 100 resamples was averaged and used. For

example, for the 1 octave FM sweep stimulus, we played 100 sweeps/direction and 20

sweeps/speed at each frequency range, resulting in a total of 800 trials (400 per direction, 80

per speed, 100 per frequency range). Therefore, when we performed decoding analyses for

frequency range, speed, and direction in the one-octave sweep condition, we used 80

trials/feature to decode each class (direction, speed, frequency range). Plots from SVM analyses

were made using the 'matplotlib' and 'seaborn' packages in Python, and accuracy scores for

points on the same axes are always directly comparable (had the same number of trials/class in

the model).

To determine if the decoding model performed above chance in individual neurons,

accuracy scores for true data were compared to accuracy scores for the model tested and

trained on data with shuffled class labels. To obtain the accuracy scores for shuffled data, class

labels were shuffled 100 times and the SVM was fit to the shuffled data each time. The mean

and standard deviation from the distribution of shuffled accuracies was calculated for each cell.

The z score for the model accuracy was calculated with reference to the shuffled distribution,

and the accuracy of the model was considered above chance if this value exceeded 1.96, (the

95% confidence interval of a standard distribution with $\mu = 1$, $\sigma = 1$).

Comparison of decoding from spike train features

To compare decoding accuracy for FM sweep features across varying dimensions of the

spike train, we calculated the distribution of the inter-spike intervals and first spike latency for

each trial. To calculate the inter-spike interval, we calculated the time between each of the

spikes and binned this distribution using 100 bins, meaning the model inputs were 100 features.

To calculate the first spike latency, we assumed a 5 ms delay to the IC (Felix et al., 2019) and

used the first spike that occurred ≥ 5 ms after the stimulus began.

Pseudo-population decoding

To examine how groups of IC neurons encode complex sound features, we evaluated

decoding accuracy in pseudo-populations of IC neurons consisting of 2-20 cells. First, we

examined coding in an individual neuron, as described above. Next, we randomly sampled 10

neurons from our population and paired each of these neurons individually with the first

neuron. To evaluate decoding for neuron pairs, we horizontally concatenated the time-binned

spike counts (rows) for each neuron pair for trials with matched stimuli and then evaluated the

performance of the model on the concatenated data. To find the overall accuracy for the

individual cell plus a paired cell, we averaged the model accuracy for each pairing. We repeated

this process with every cell in our dataset, pairing it with 10 randomly selected neurons and

evaluating average model accuracy across the 10 pairs to get an overall paired accuracy for the

population.

We next continued this process by increasing the number of paired cells for each

individual neuron the dataset. For each individual cell, there were 10 randomly selected groups

of neurons that were paired (e.g., 10 groups of 2, 3, 4, 5... etc.) and decoding was performed on

the concatenated time-binned spike counts from these groups. For each cell, the average

accuracy from each set of pairings was calculated, and then the average accuracy across the

dataset was plotted.

Statistical tests

All statistical tests were performed using Python 3.11.9. To evaluate whether there was

significant decoding accuracy in individual neurons, we z-scored accuracies relative to shuffled

class accuracy distributions, as described above. To evaluate whether there were differences in

decoding accuracy between true and shuffled bin conditions, data were evaluated using a

paired t-test ('ttest_rel' function from 'scipy.stats'). To examine correlations between decoding

for sound features, we performed a linear regression.

To examine direction decoding accuracy across other varying sweep parameters such as

sweep intensity and speed, a repeated-measures ANOVA ('ANOVArm' from

'statsmodels.stats.anova') was performed followed by Tukey's HSD post-hoc tests

('pairwise_tukeyhsd' from 'statsmodesl.stats.multicomp') where appropriate. We also used a

repeated-measures ANOVA and Tukey's HSD post-hoc test to examine if increasing the number

of cells in each pseudo-population increased the average accuracy. To test for an increase in the

number of cells that significantly encoded direction over increasing speed or intensity, we used

a Chi-square test for trend ('chi2_contingency' from 'scipy.stats'), which can be used to examine

changes in proportions over ordered groups.

All p-values were compared to a Bonferroni-corrected α value for evaluation of

significance where appropriate, and in some cases Bonferroni-adjusted p-values are instead

displayed and noted as "adj. p-value".

Direction selectivity index calculation

The direction selectivity index (DSI) was calculated as follows, where $spikes_{up}$ indicates

the number of spikes that occurred during upward frequency sweeps and $spikes_{down}$ indicates

the number of spikes that occurred during downward frequency sweeps:

$$DSI = \frac{spikes_{up} - spikes_{down}}{spikes_{up} + spikes_{down}}$$

751   The time window across which spikes were summed for the 4-octave frequency sweeps

752   was 480 ms after stimulus onset (since the longest stimulus was 400 ms, this is stimulus time +

753   20% of stimulus time to account for any offset spiking that may be directionally selective). This

754   is the same time window over which spike times were binned for the machine learning analysis.

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Table 1. Stimuli used for in vivo electrophysiological recordings

Stimuli	Frequency range (kHz)	Intensity (dB SPL)	Speeds (octaves/sec)	Repeats
1 octave FM sweeps	4-8 8-16 16-32 32-64	70	10-200	10
2 octave FM sweeps	4-16 8-32 16-64	70	10-200	10
4 octave FM sweeps	4-64 at 5 steps/octave	10, 30, 50, 70	10-200	5
Pure tones (200 ms)	4-64 at 5 steps/octave	-100, 10, 30, 50, 70	N/A	5
Vocalizations	N/A	70 dB	N/A	10

912   All FM sweeps are logarithmic.

914 **Table 2. Idealized bin sizes and number of bins used for analysis.**

Stimuli	Stimulus duration (ms)	Binned duration (stimulus + 20%)	Num. bins that resulted in highest decoding accuracy	Bin size (ms) that resulted in highest decoding accuracy	Num. bins used in analysis	Bin size (ms) used in analysis
4 octave FM sweeps	400	480	55	8.7	209	2.3
2 octave FM sweeps	200	240	75	3.2	104	2.3
1 octave FM sweeps	100	120	51	2.3	51	2.3

Bin sizes and number of bins used for analysis. We first calculated the idealized bin sizes for

machine learning model. To determine the best bin size to use for the decoding model, we

trained the SVM to decode direction in 1, 2, and 4 octave sweeps from neuron time-binned

spike counts binned using 1-501 bins in steps of 2 bins. The listed values are the bin sizes that

yielded the highest direction decoding accuracy for each stimulus. Next, we calculated the

number of bins needed for each stimulus to maintain a consistent time window (2.3 ms) over

which each of the trials were binned. Because the 1, 2, and 4 octave stimuli were different

lengths (sweep speeds were conserved across stimuli), this resulted in a different number of

bins for the 4, 2, and 1 octave FM sweep stimuli.

Figure 1. IC neurons use spike timing to encode direction information for FM sweeps

A, Experimental design. Awake mice were headfixed in a sound booth with sound presented to

the right side of the mouse while juxtacellular recordings were performed in the left IC. *B,*

Example of a DiI labeled recording site in the left IC, outlined in white. *C,* The tonal receptive

field at 70 dB SPL for each neuron included in the study, sorted by best frequency. *D,* Four

example neuron responses to the slowest (10 octaves/s) up (top row) and down (bottom row)

frequency-modulated (FM) sweeps. Grey boxes indicate when the sound was presented. *E,*

Raster plots showing responses to four-octave FM sweeps for neurons shown in *D*. The top half

of the plot shows responses to upward sweeps, and the bottom half of the plot shows

responses to downward sweeps. Sweep speed varies along the y-axis with the fastest sweep

speed shown at the middle of the y-axis (200 octaves/s) and sweep speeds becoming

progressively slower toward the top and bottom of the y-axis. *F,* Frequency response areas

(FRAs) for neurons shown in *D.* FRAs were constructed using 200 ms tone pips presented in

pseudorandom order to cover a 4-64 kHz frequency range at 5 steps/octave intervals and the

listed intensities. The bottom row of the heatmap indicates the spontaneous firing rate of the

neuron. *G,* Example of a hyperplane from a model trained to decode direction from neural spike

time data. For visualization purposes, data were binned into 16 bins and then PCA-transformed

and projected onto the first two principal components. Colored regions on each side of the

hyperplane indicate the margins. *H,* Direction decoding accuracy scores for 4-64 kHz FM

sweeps. Blue bars indicate accuracy scores for model trained on true data; orange bars indicate

accuracy for model trained on data with shuffled class labels. *I,* Histogram of direction

selectivity indices (DSIs) calculated from the same group of cells shown in *H.* The histogram is

overlaid with a kernel density estimate that was generated using the 'kde' argument for

seaborn's 'histplot' function. *J,* Scatterplot comparing the accuracy of the model for decoding

direction and the absolute value of the DSI in individual neurons. Blue dots are true accuracy,

orange dots are accuracy of the model with shuffled class labels. Grey line shows the linear

regression between true accuracy labels and DSI, indicating no correlation between the two

values. Vertical orange line is the DSI cutoff from Kuo and Wu (2012); neurons to the right of

this line are considered direction selective according to the DSI metric. Horizontal orange line is

model chance. *K,* Comparison of model accuracy for direction decoding with time bins in correct

order vs. shuffled time bins. Class labels are maintained in each case. Individual neurons are

connected by lines, and the mean is shown in dark blue. *L,* Scatterplot showing the accuracy for

true bin order vs. shuffled bin order (same as *K*). The dashed grey line indicates the line of

identity (x = y).

Figure 2. Four-octave FM sweep direction decoding is consistent across varying speeds but not intensities

A, Sample traces from a recording showing differing responses to four-octave up and down sweeps (10 octaves/second) at each intensity level. Sound presentation is indicated by the grey box. *B,* Accuracy of direction decoding across varying sweep speeds. The blue line indicates direction decoding accuracy across speeds for true labels, and the orange line indicates accuracy for shuffled labels (chance). The standard deviation is shown with shading. *C,* Heatmap showing Tukey HSD p-values for each pairwise comparison of true data accuracy scores for each speed in *B.* Lighter colors indicate more significant results. No comparisons were statistically significant. *D,* Accuracy of direction decoding across varying sweep intensities. The blue line indicates direction decoding accuracy across intensities for true labels, and the orange line indicates accuracy for shuffled labels (chance). The standard deviation is shown

975   with shading. *E,* Heatmap showing Tukey's HSD p-values for each pairwise comparison of true

976   data accuracy scores for each speed in *D.* Lighter colors indicate more significant results.

977   Decoding accuracy at 70 dB SPL was significantly higher than accuracy at 10 dB SPL (Tukey's

978   HSD, p = 0.0001); this is indicated with an asterisk.

Figure 3. IC neurons encode frequency range, speed of one- and two-octave FM sweeps

A, Raster plots with responses to one-octave FM sweeps of varying sweep frequency ranges

(listed on top of each plot). Up sweeps occupy the top half of the plot and down sweeps occupy

the bottom. Slowest speeds are on the outsides with fastest speeds in the middle. Sound onset

is shown by the orange line at 100 ms. ***B,*** Raster plots showing responses from the same neuron

in *A* to the two-octave FM sweeps, played at the same speeds. ***C,*** Direction, speed, and

frequency range decoding accuracy for one-octave FM sweeps. True accuracy is shown in blue,

accuracy with shuffled bins is in orange. Chance for each plot is shown with a grey dashed line.

D, Decoding accuracies for the same sound features shown in *C,* for two-octave FM sweeps. **E,**

Model predictions (x-axis) versus actual (y-axis) categories for decoding of each sound feature.

Predictions are aggregated across all neurons in the dataset. Chance performance is white,

while above chance is red and below chance is blue. **F-G,** Same as A, for speed and frequency

range decoding for one-octave sweeps. **H-J,** Same as *E-G* for decoding from two-octave sweeps.

Figure 4. IC neurons multiplex features of one- and two-octave FM sweeps

A, Scatterplots showing correlations between feature encoding accuracies in individual cells for one-octave FM sweeps. Models trained on true class labels are shown in blue and models trained on shuffled class labels are shown in orange. R-squared and p-values from linear regressions between true data points for feature pairs are shown on each plot. For six total comparisons, the Bonferroni-corrected significance level (α) = 0.0083. *B,* Correlations of feature decoding accuracies in individual cells as in *A* for two-octave FM sweeps.

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Figure 5. IC neurons use multiple strategies to encode FM sweep features in a single spike

train

A, Accuracies for decoding direction in one-octave sweeps from models trains on the time-

binned spike counts, the distribution of inter-spike intervals (ISI), or first spike latency (FSL) in

individual cells (blue points) compared to shuffled data (orange points). *B-C,* Same as *A*, for

speed and frequency range. *D,* Correlation between decoding accuracy in models trained on

time-binned spike counts or ISIs for direction in one-octave FM sweeps. *E-F,* Same as *D,* for

speed and frequency range. *G-L,* Same as *A-F,* for two-octave sweeps.

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Figure 6. Spike timing is a critical component of feature encoding for one- and two-octave FM

sweeps

A, Left panel: comparison of accuracy scores for decoding sweep direction for one-octave FM

sweeps across each neuron where the bin order is intact (True) and shuffled (Shuffle). Class

labels are maintained by trial in both cases. The mean is shown in dark blue, and light blue lines

represent individual neurons. Right panel: scatterplot comparing accuracy with true bin order

and shuffled bin order in individual neurons. The line of identity is shown in dashed grey (x = y).

B-C, same as *A* for speed and frequency range encoding across true and shuffled bin data for

one-octave FM sweeps. *D-F*, same as *A-C* for two-octave FM sweeps.

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Figure 7. IC neurons encode FM sweep features over different time scales relative to stimulus onset

A, Direction decoding accuracy across time (6.9 ms time bins) for one-octave FM sweeps. The blue line indicates decoding accuracy for data with true labels, and the orange line indicates decoding accuracy for data with shuffled labels. Shading around each line represents the standard error of the mean. The dashed black line marks stimulus onset (100 ms). *B-C,* Same as *A* with speed and frequency range decoding across time for one-octave FM sweeps. *D,* Overlay

1033   of accuracy scores from *A-C* normalized to their relative pre-stimulus values. ***E-G,*** Same as *A-C*

1034   for two-octave stimuli. ***H,*** Same as *D* for two-octave stimuli.

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Figure 8. Pseudo-populations of IC neurons provide higher decoding accuracy compared to individual neurons

A, Left: Direction decoding accuracy of each neuron in the one-octave dataset paired with 1-20 additional neurons. Each light blue line represents decoding from one seed neuron, and the dark blue line represents the mean at each pseudo-population size. Orange lines show accuracy scores from decoding with class labels shuffled. Right: Tukey's HSD post-hoc test corrected p-values from pairwise comparisons between the true accuracy of each pseudo-population size. Light squares represent significant comparisons while dark squares indicate comparisons that were not significantly different from each other. *B-C,* Same as *A* for speed and frequency range decoding. *D-F,* Same as *A-C* for two-octave FM sweeps.

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Figure 9. IC neuron responses to vocalizations do not depend on frequency sweep direction

A, Spectrograms of four example vocalizations (one from each class) used as stimuli. *B,*

Decoding accuracy for vocalization class in individual IC neurons (blue) compared to decoding

from shuffled classes (orange). Chance is labeled with a grey dashed line at 25%. *C,* Decoding

accuracy for the true direction of the frequency sweep contained in the vocalization. *D,*

Decoding accuracy for the vocalization class regardless of whether the stimulus was played

forward or backward. *E,* Example peristimulus time histograms for the response from one

neuron to each of the example upsweep vocalizations and downsweep vocalizations. Response

to the forward vocalization is in pink and response to the backward vocalization is in yellow. The

black bars indicate the sound presentation window. *F,* The frequency response area for the

neuron in *E,* constructed from responses to 5 presentations each of 200 ms pure tones at 4

intensities and over 4 octaves with 5 frequency steps/octave. Spontaneous firing is shown in the

bottom row. *G,* Frequency response areas from neurons where vocalization type (up/down)

could be decoded significantly above chance.

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