Limitations of Dynamic Causal Modelling for Multistable Cortical Circuits

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Abstract

Dynamic causal modelling (DCM) has been used extensively for inferring effective connectivity from neuroimaging data. However, it is unclear whether the DCM approach can reveal neural circuits with multistable dynamic states with global dynamical structures. In this work, we used excitatory-inhibitory cortical columnar neural mass models endowed with multistable dynamical states as ground truths to evaluate whether DCM can accurately identify their models' architecture and connectivity strengths. Specifically, we simulated three recurrently connected neural mass models with different types of multistability, and generated local field potential data for DCM. The first model has bistable fixed points and exhibiting binary decision-making behaviour, and the second model has co-existence of two stable oscillatory frequencies (period doubling). The third model exhibits deterministic chaos, with a continuum of confined states. For each of the three models, DCM's Bayesian model selection was able to correctly identify the correct model architecture among various options in model space. However, DCM's Bayesian model averaging of the winning model was unable to accurately elucidate all the models' extrinsic connectivity strengths, leading to the behaviours of the reconstructed models to differ substantially from their corresponding ground-truth models. Further, we found DCM's estimation was highly sensitive to the sampling frequency used during its training. Overall, this work reveals the limitations of DCM in evaluating complex, multistable neural dynamical states and hence caution its use under these conditions.

1. Introduction

Elucidating the functional and effective connectivity of healthy or dysfunctional brains is one of the aims in neuroscience (Friston, 2011). In particular, network-based neuroscience offers opportunities to provide deeper understanding of the principles and mechanisms underlying complex brain function and cognition (Bassett and Sporns, 2017). Functional and effective connectivity analyses are often conducted in human studies using non-invasive functional neuroimaging such as electroencephalography (EEG), magnetoencephalography (MEG), and functional magnetic resonance imaging (fMRI) (Friston, 2011). In animal or certain drug treatment resistant clinical patient studies, functional and effective connectivity are applied to invasive intracranial/stereo EEG (i/sEEG) (e.g., Kobayashi et al. (2024)), local field potential (LFP) (e.g., Gallego-Carracedo et al. (2022); Meyer et al. (2018)) and multi-neuronal activity data (e.g., Tang et al. (2024); Trepka et al. (2022)).

Effective connectivity provides additional directed connectivity information than functional connectivity (Friston, 2011) and is often state-space model dependent, for example, requiring the use of autoregressive models in Granger causality (Granger, 1969), or nonlinear neural cortical models in dynamic causal modelling (DCM) (Friston et al., 2003). In particular, DCM has been successfully applied to a variety of neuroimaging studies, not only in elucidating effective network connectivity but also inferring the underlying neural substrates for cognitive functions or dysfunctions (Huang and Nam, 2020).

The models in DCM are based on the principle of canonical cortical columns (Mountcastle, 1997). DCM's comparison and selection of potential models and estimation

of extrinsic connectivity between columns are based on Bayesian statistical methods (Penny et al., 2011). Specifically, variational Bayes, under the Laplace assumption, is made, and model estimation including network connectivity strength requires the maximisation of a quantity called the negative variational free energy (Friston et al., 2007). However, the Laplace's approximation, which provides an analytical expression for a posterior probability distribution by Gaussian distribution fitting, is symmetric around the distribution mode and is derived locally (Friston et al., 2007). Thus, it is unclear how well DCM can be applied to complex or global neural dynamical states, such as those comprising multiple stable states.

In this study, we investigate how DCM can accurately elucidate the model architecture and the extrinsic connectivity strengths of neurophysiologically based cortical column models with multistable states. Specifically, we investigate the performance of DCM on neural activities generated from computational models with: (i) bistable stable steady states (fixed points; i.e. choice attractors for decision-making (e.g. Roach et al. (2023a); Roxin and Ledberg (2008); Wong and Wang (2006)); (ii) two stable neural oscillatory frequencies (i.e. period-doubling condition) (Jia et al., 2012); and (iii) the extreme case where there is a finite continuum of multistable states i.e. deterministic chaos (Strogatz, 2018). Importantly, these specific neural dynamics are investigated as they are not only physiologically plausible (Breakspear, 2017) and can be generated from cortical column models, but they are also not determined by local dynamics about some steady state. These models will be used as ground truths to compare with the elucidated DCM models, while maintaining the same intrinsic connectivity.

Our results show that although DCM can correctly identify the correct models' architecture within the model space, the winning model has connectivity strengths that deviate substantially from those in the corresponding ground-truth models. Thus, our work demonstrates the limitations of current DCM approach.

2. Methods

2.1. Cortical columnar neural mass models

To evaluate DCM, we made use of local field potential (LFP) data generated from three different types of multistable neural mass models, which act as ground truths. In particular, all the models were based on cortical columnar structure conforming to DCM (Fig. 1).

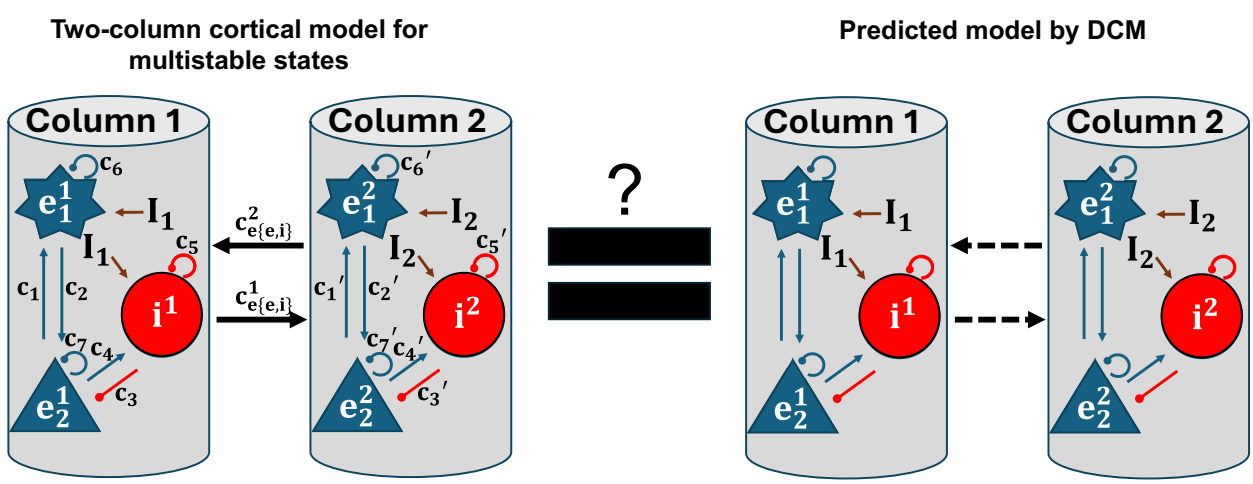

Fig. 1. Schematic of DCM testing. To test whether the between-column (extrinsic) connections in multistable cortical circuit models (left) can be recovered by DCM-inferred models (right) in terms of model architecture identification and connectivity strengths based on the generated local field potential data from ground-truth models.

2.1.1. Model with bistable fixed points that exhibits decision-making behaviour

The model with bistable fixed points for decision making comprised a two-column cortical neural mass model with two excitatory (e_1 and e_2) and one inhibitory (i) neural populations, lateral connectivity between columns and fully self-feedback, as described by Youssofzadeh et al. (2015).

We represented the stimulus input to both columns using a Gaussian bump function (Friston, 2008):

$$u_1(t) = (a + \Delta) * e^{\frac{-(t-t_0)^2}{\Delta t^2}} \quad (1)$$

$$u_2(t) = (a) * e^{\frac{-(t-t_0)^2}{\Delta t^2}} \quad (2)$$

Here, a represents the amplitude at zero bias (Δ), with t_0=0 s as the stimulus onset time and t=2 s as the stimulus offset time. The parameter Δt (0.007 s) determines the width of the Gaussian bump.

Moreover, we define the evidence quality ε (analogous to motion coherence in random dot kinematogram) as follows:

$$\varepsilon = \frac{u_1(t_0) - u_2(t_0)}{u_1(t_0) + u_2(t_0)} \quad (3)$$

Noise is introduced to the excitatory (e_1) and inhibitory (i) populations through the inputs I_η filtered via the fast synaptic activation of AMPA receptors. The dynamics of this process are described by the following equation (Wong and Wang, 2006):

$$\frac{dI_\eta}{dt} = -\frac{I_{\eta 1}}{\tau_{\text{AMPA}}} + \frac{\eta(t)}{\sqrt{\tau_{\text{AMPA}}}} \quad (4)$$

where τ_{AMPA} is 5 ms, and $\eta(t)$ is a white Gaussian noise with zero mean and a standard deviation of 0.02 nA. Then the total input current to each of the columns is:

$$I(t) = u(t) + I_{\eta}(t) \tag{5}$$

The network parameters were set to simulate two-alternative decision-making and working memory-based storage of the made decision via multistable dynamics as observed via PSP of e_1 with respect to input current using XPPAUT (Ermentrout and Mahajan, 2003). For DCM, we adjusted the input to the first column to be 50% greater than the input to the second column. We then categorised the trials into three types: (i) correct trials, where the output of the first column was significantly higher ($e_1^1 > e_1^2$) and reaching a decision threshold during stimulus; (ii) error trials, where the output of the second column was higher and reaching a decision threshold ($e_1^2 > e_1^1$); and (iii) 'non-decision' trials, where the output difference between the two columns did not meet the decision threshold.

Within this model, the neural population's mean firing activity function S, which resembles a sigmoidal curve, represents the post-synaptic potentials and described by:

$$S(v) = \frac{1}{1 + \exp(-r_1(v - r_2))} - \frac{1}{1 + \exp(r_1 r_2)} \tag{6}$$

The parameters r_1 and r_2 of the sigmoidal function influence its shape; increasing r_1 decreases the slope's steepness, while increasing r_2 moves the curve to the right. The mean firing rate, derived from the average membrane depolarization (or PSPs) through a static nonlinear sigmoidal function. Table S1 presents the priors and physiological meanings of the model parameters.

According to schematic Fig. 2A, there is a lateral connection from neuron e_2 in column one to neuron e_1 in column two and vice versa. Moreover, there is a lateral connection from neuron e_2 in column one to neuron i_1 in column two and vice versa.

Thus, a system of differential equations describing the two-column cortical model, according to Fig. 2, can be defined in the following.

For cortical column j (the other column labelled as k):

Post-synaptic potential for e_1^j:

$$\dot{v}1_j = y1_j \tag{7}$$

$$\dot{y}1_j = H_e K_e[c_1 \mathrm{S}(v2_j - v3_j + v7_j) + c_{ee}^k \mathrm{S}(v2_k - v3_k + v7_k) + I_j] - 2K_e y1_j - K_e{}^2 v1_j + I_j \tag{8}$$

Post-synaptic potential for e_2^j:

$$\dot{v}2_j = y2_j \tag{9}$$

$$\dot{y}2_j = H_e K_e[c_2 \mathrm{S}(v1_j + v6_j)] - 2K_e y2_j - K_e{}^2 v2_j \tag{10}$$

$$\dot{v}3_j = y3_j \tag{11}$$

$$\dot{y}3_j = H_i K_i[c_3 \mathrm{S}(v4_j - v5_j)] - 2K_i y3_j - K_i{}^2 v3_j \tag{12}$$

Post-synaptic potential for i^j:

$$\dot{v}4_j = y4_j \tag{13}$$

$$\dot{y}4_j = H_e K_e[c_4 \mathrm{S}(v2_j - v3_j + v7_j) + c_{ei}^k \mathrm{S}(v2_k - v3_k + v7_k) + I_j] - 2K_e y4_j - K_e{}^2 v4_j + I_j \tag{14}$$

Post-synaptic potential due to self-inhibition for i^j:

$$\dot{v}5_j = y5_j \tag{15}$$

$$\dot{y}5_j = H_i K_i[c_5 \mathrm{S}(v4_j - v5_j)] - 2K_i y5_j - K_i{}^2 v5_j \tag{16}$$

Post-synaptic potential due to self-excitation for e_1^j:

$$\dot{v}6_j = y6_j \tag{17}$$

$$\dot{y}6_j = H_e K_e[c_6 \mathrm{S}(v1_j + v6_j)] - 2K_e y6_j - K_e{}^2 v6_j \tag{18}$$

Post-synaptic potential due to self-excitation for e_2^j:

$$\dot{v}7_j = y7_j \tag{19}$$

$$\dot{y}7_j = H_e K_e[c_7 \mathrm{S}(v2_j - v3_j + v7_j)] - 2K_e y7_j - K_e{}^2 v7_j \tag{20}$$

The LFP for column j is defined as (Mazzoni et al., 2015):

$$LFP_j = EPSP_j + IPSP_j = y1_j + y2_j - y3_j + y4_j - y5_j + y6_j + y7_j \tag{21}$$

2.1.2. Models with period doubling and deterministic chaos

During period-doubling and chaotic regimes, we used three network architectures for DCM estimation to reveal distinct modes of cortical connectivity, such as decision-making bistability (Fig. 3A-C). To model the ground truth, we employed the model proposed by Ghorbani et al. (2012) to simulate the cortical column during period-doubling and chaotic regimes (Fig. 3A). However, due to the limitations of DCM in estimating synapses with temporal dynamics in the SPM12 toolbox (Penny et al., 2011), the adaptation for connections from excitatory-to-excitatory neurons is omitted.

In this model, each neural population averaged membrane potential V_m follows standard rate equation, where m denotes either excitatory (e) or inhibitory (i) neural population:

$$\frac{dV_m}{dt} = -\frac{V_m}{\tau_m} + \sum_n c_n\, r(V_m) + I \tag{22}$$

In this equation, the first term on the right-hand side describes the relaxation of the membrane potential to equilibrium. The membrane time constants τ_e (20 ms for excitatory neurons) and τ_i (10 ms for inhibitory neurons) represent the rate at which the membrane potential returns to its resting state after being depolarised or hyperpolarised (Bal and Destexhe, 2009). The second term represents the changes in membrane potential due to excitatory post-synaptic potentials (EPSPs) and inhibitory post-synaptic potentials

(IPSPs), where the sum runs over all neural populations connected to neural population n. Here, $r(V_m)$ is the firing rate of neural population m, and c_n represents the connectivity strength between neural populations.

A neural population's firing rate is determined by its membrane potential, which follows a sigmoidal curve as modelled by the following equation:

$$r(V_m) = \frac{r_1}{1+ exp(\frac{-(V_m - V^*)}{g_m})} + r_0 \tag{23}$$

Here, $r_1 = 70$ Hz is the maximum firing rate, V^* is the firing threshold, and g_m controls the steepness of the rate dependence on membrane potential. We assume that $g_e > g_i$, meaning that (e.g. fast-spiking) inhibitory neural populations have steeper firing rates in response to changes in membrane potential. In our simulations, we set $g_e = 5$ mV and $g_i = 2$ mV.

The model architecture for period-doubling and chaos comprises a two-column cortical neural mass model that includes two excitatory (e_1 and e_2) and one inhibitory (i) neural population, lateral connectivity between columns, and fully self-feedback connections. The nonlinear interaction between these two columns underpins period-doubling and chaos. Then the dynamics of the system are governed by three dynamical variables: the common membrane potential of excitatory neurons V_{e1} *and* V_{e2}, the common membrane potential of inhibitory neurons V_i. Their evolution is described by the following rate equations.

For cortical column j (the other column labelled as k):

$$\frac{dV_{e1}^{j}}{dt} = -\frac{V_{e1}^{j}}{\tau_e} + c_6\, r(V_{e1}^{j}) + c_1\, r\left(V_{e2}^{j}\right) + I_j \tag{24}$$

$$\frac{dV_{e2}^{j}}{dt} = -\frac{V_{e2}^{j}}{\tau_e} + c_7\, r(V_{e2}^{j}) + c_{ee}^{k}\, r(V_{e2}^{k}) + c_2\, r(V_{e1}^{j}) - c_3\, r(V_{i}^{j}) \tag{25}$$

$$\frac{dV_{i}^{j}}{dt} = -\frac{V_{i}^{j}}{\tau_i} + c_4\, r(V_{e2}^{j}) + c_{ei}^{k}\, r(V_{e2}^{k}) - c_5\, r\left(V_{i}^{j}\right) + I_j \tag{26}$$

Tables S2 and S3 present the priors and physiological meanings of the model parameters during period-doubling and chaos.

In this model, since the definitions of EPSP and IPSP are not as straightforward as those in the decision-making model, we follow the methodology of Azimi et al. (2021) and define the LFP for each column as (- V_{e2}).

2.2. DCM estimation of models

Based on our alterations of intrinsic and extrinsic connections in the models, we modified the event-related potential (ERP) based DCM equations in the SPM12 toolbox (Penny et al., 2011) to match our revised cortical columnar formulas similar to Youssofzadeh et al. (2015). Specifically, for bistable decision-making model, we modified the state equations and prior moments for ERPs and leadfield parameters according to equations (1-(21 and Table S1. For period-doubling and deterministic chaos dynamics, we modified state equations and prior moments according to equations (22(26, Table S2, and Table S3. Importantly, due to the constraint in that the current SPM toolbox does not allow separate extrinsic lateral connections for excitatory and inhibitory populations, we implemented a workaround for the chaos regime by incorporating the ratio between excitatory and inhibitory lateral connection strengths. Specifically, we adjusted the lateral connections by scaling the inhibitory-to-inhibitory connection strengths within the SPM toolbox by a

factor matching the ratio between excitatory and inhibitory connections informed from the ground-truth.

Based on the generated LFP, which estimates the neural population activities in the source (Penny et al., 2011), we first applied DCM based on three different possible models in model space. The first model was the ground-truth model with lateral connectivity between cortical columns (Fig. 2A and Fig. 3A) whereas the second model assumed the forward-backward connectivity between the columns (Fig. 2B and Fig. 3B) (with no modulatory connections). The third model is the fully connected model with both lateral and forward-backward connectivity (Fig. 2C and Fig. 3C).

2.3. Statistical analysis

2.3.1. Bayesian model selection

After the DCM estimation in the model space separately for each trial, a Bayesian model selection (BMS) (Stephan et al., 2009; Wasserman, 2000) identified the winning model using the random effects (RFX) procedure (Penny et al., 2011). We selected the RFX approach with the assumption of different performance mechanisms for different trials (Austin, 2011). This method calculates the model probabilities which are described by a Dirichlet distribution and the optimised Dirichlet density using the observed data and variational Laplace approach can compare the models at a group level (Stephan et al., 2009). Considering each model's estimated posterior distribution given the observed data, one can utilise the Bayesian model averaging (BMA) strategy to calculate the average over all models by averaging the posterior distributions of models weighted by their posterior model probability (Trujillo-Barreto et al., 2004; Woolrich et al., 2009).

2.3.2. Bayesian model averaging

To estimate the averaged extrinsic connectivity strengths for each condition, we performed BMA on the estimated DCMs of the winning model (Penny et al., 2011). This approach combines the parameter estimates from trials, weighted by the posterior probability of each model, to account for model uncertainty and provide robust averaged estimates.

2.3.3. Reconstructed neural activity from DCM estimation

We simulated neural activity using estimated connectivity strengths of the winning model in BMS instead of the connectivity strengths in ground-truth models. For the bistable decision-making case, psychophysical metrics (decision accuracy and normalised decision time) were evaluated using simulations based on connectivity estimates obtained from correct and error trials combined. This combined-trial approach was eventually chosen because it has been demonstrated that decision-making models recover ground-truth parameters more effectively when using both correct and error trials, compared to when using either trial type alone (Asadpour and Wong-Lin, 2024). For period-doubling and chaos regimes, we reconstructed and plotted the network activity timecourses and phase-space trajectories using the estimated BMA connections. For period-doubling and chaotic regimes, the Lyapunov exponents (Strogatz, 2018) were computed.

2.4. Numerical method, and data and code availability

In numerical simulations, all the models' nonlinear equations were solved using Euler method, in MATLAB R2023b software with a time step of 1 millisecond (smaller time step did not affect the results). For simulations using stochastic differential equations, we used

the same set of pseudo-random seed when comparing between the generated data of the ground-truth models and corresponding DCM-estimated models, akin to Lenfesty et al. (2025).

Simulations of models exhibiting bistable fixed points, period-doubling, and deterministic chaos were performed on a laptop with an Intel® Core™ Ultra 7 155H processor (1.40 GHz), 64.0 GB LPDDR5x memory (Dual Channel, 6400 MT/s), a 1 TB M.2 PCIe NVMe solid-state drive, NVIDIA® GeForce RTX™ 4050 graphics card (6 GB GDDR6, 30 W), and Windows 11 Enterprise operating system.

For DCM estimation, BMS, and BMA, computations were performed using MATLAB R2022a software via the Northern Ireland High-Performance Computing (NI-HPC) facility (https://www.ni-hpc.ac.uk). Additionally, figures were generated on another device equipped with an Intel(R) Core™ i7-7700 CPU processor (3.60GHz), 32.0 GB RAM, and 64-bit Windows 10 Enterprise operating system.

3. Results

3.1. Cortical columnar model with multistable fixed points for decision making

We present a two-column cortical neural mass model that includes self-feedback (Youssofzadeh et al., 2015) and exhibits multistable fixed points for two-alternative decision-making (Roach et al., 2023b; Wong and Wang, 2006).

We initially considered the input to two cortical columns to be random, assuming equal stimulus inputs in the form of Gaussian bumps (see Methods). In subsequent stages, we gradually increased the input Gaussian bump to one of the cortical column (column one) relative to the other cortical column (column two). A decision is considered

made when the activity of one of the neuronal populations surpasses the threshold. By considering the model's activity output, we observe three different types of simulated trials for various levels of inputs: correct trials, error trials, and non-decision trials (see Methods) (Fig. 2A and S1). Correct (error) trials occur when the cortical column that receives a higher (lower) stimulus input, that is column one (two), has its excitatory neural population reaches a prescribed decision activity threshold first, towards one of the two stable fixed points (a choice attractor (Roach et al., 2023b; Wong and Wang, 2006)). Non-decision trials occur when none of the cortical columnar activities reach the decision threshold during stimulus presence.

The overall behaviour of the model recapitulated stereotypical psychophysics in two-choice reaction time experiments (Fig. 2D). Notably, the neural activity of the winning neuronal population exhibits a faster ramp-up with higher evidence quality (ε). Fig. 2E depicts the evolution of neural activity across different input strengths (ϵ), with the decision threshold clearly delineating the onset of the response. Correspondingly, accuracy improves monotonically with increased evidence quality (Fig. 2F), while decision time decreases, with error decisions being slower than correct ones; typical speed-accuracy trade-off (Fig. 2F; Kaufman et al. (2015); Roitman and Shadlen (2002); Shadlen and Newsome (2001)).

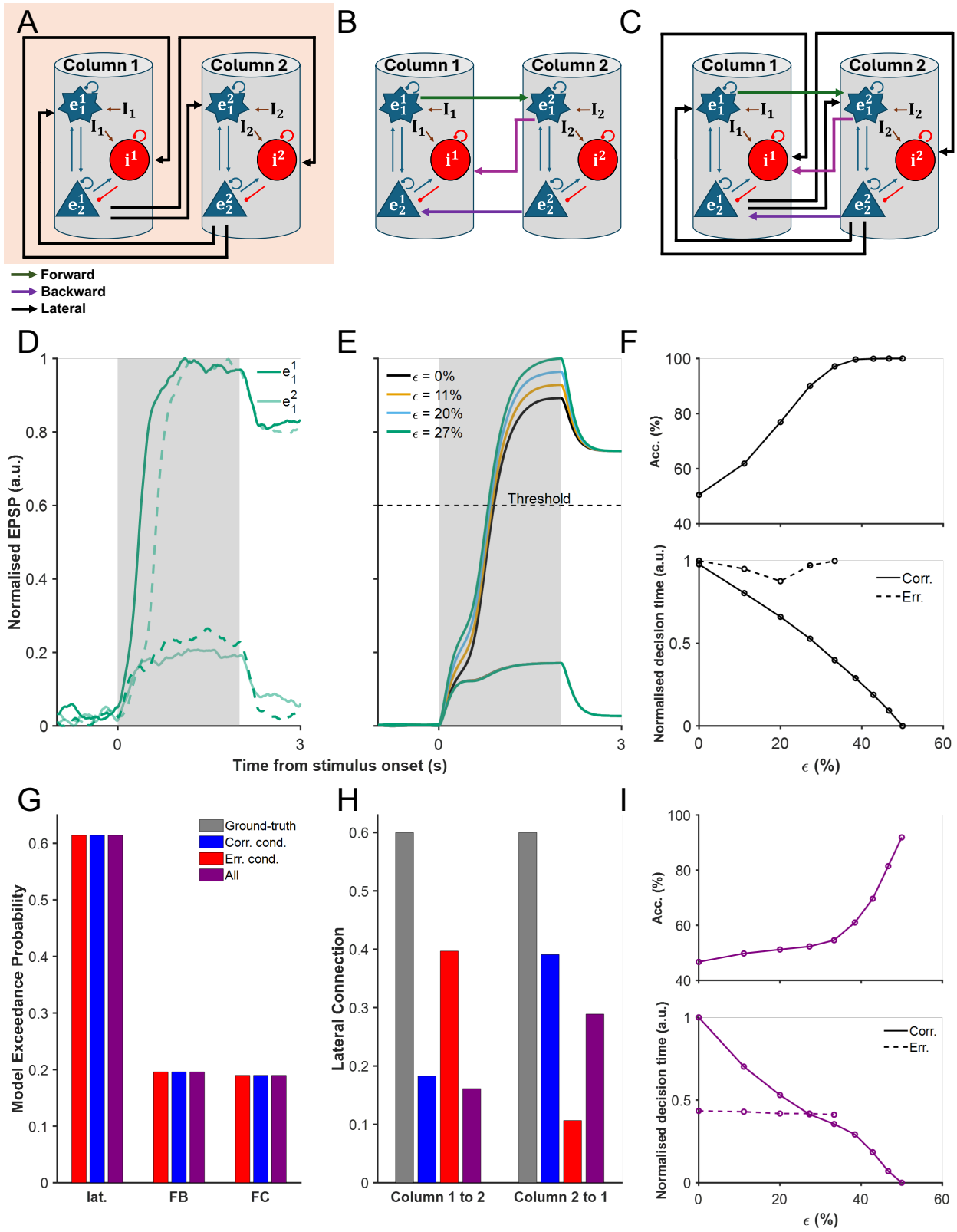

Fig. 2. Evaluation of DCM's ability to recover multistable cortical circuit dynamics. (A) Illustration of the ground-truth model, which incorporates only lateral (lat.) excitatory

and inhibitory connections between cortical columns. (B) Alternative model featuring only forward-backward (FB) connections. (C) Fully connected (FC) model that includes both lat. and FB connections. (D) Simulated neural activity timecourse of e_1 from the laterally connected model (A), with the output for column 1 (e_1^1) and column 2 (e_1^2) plotted separately. Solid (dashed) lines: correct (error) trials. (E) Neural activity timecourse across different input strengths (ϵ), with a decision threshold demarcating decision time. (F) Psychophysical performance of the ground-truth model, where accuracy (Acc.; top) increases with input strength, while normalised decision time (bottom) decreases. (G) Bayesian model selection (BMS) results, illustrating the model exceedance probabilities across correct (Corr.), error (Err.), and combined (All) trial conditions. (H) The estimated lateral connection strengths inferred by DCM. (I) Reconstruction of accuracy and normalised decision time based on the recovered connection strengths of all-trial condition from (H).

To estimate DCM, we simulated the model across four distinct levels of evidence quality. For each level, we generated 200 correct trials and 200 error trials, resulting in a total of 400 trials per evidence quality level. This approach produced an aggregate of 1600 trials for comprehensive DCM estimation.

3.2. DCM identifies correct decision model architecture but not connectivity strengths

To evaluate the accuracy of DCM in identifying the underlying network architecture, we performed BMS across trials classified as correct, error, and all combined for the three different models in the model space with lateral connectivity, feedback connectivity, and full connectivity (Fig. 2A-C). The results show that BMS reliably identifies the ground-truth model as the most probable structure across all trial types (Fig. 2G). Notably, the exceedance probability of the model with extrinsic connections similar to ground-truth model remains significantly higher than that of the alternative models, suggesting that DCM effectively differentiates between model architectures in the given multistable cortical circuit.

While BMS successfully selects the correct model architecture, the estimated extrinsic connection strengths obtained through BMA deviate from the ground truth (Fig. 2H). Specifically, the inferred lateral connection strengths differ significantly from those in the simulated ground-truth model, suggesting that DCM struggles to recover precise network parameters. This discrepancy is particularly evident in trials where the winning model should maintain symmetric extrinsic connections, yet BMA estimates reveal noticeable asymmetries which in turn will introduce choice behavioural bias. Further, our results indicated that considering only correct or error trials alone lead to more asymmetry in connectivity strengths between columns than combining all trials.

To assess the impact of these estimation errors, we compared the psychophysical performance of the ground-truth model (Fig. 2F) with the performance reconstructed using DCM-estimated connection strengths for all trials by averaging over 1000 simulations for each evidence quality (Fig. 2I). The all-trials condition was used as it showed the least asymmetry (i.e. the best results) in connectivity between columns (Fig. 2H). When applying DCM-estimated connections from all trials, with combined correct and error trials, the reconstructed model's decision accuracy deviated from that of the original model especially for intermediate evidence quality levels. Specifically, while the general trend was similar, the reconstructed accuracy curve differed in shape from the ground-truth, displaying a positive second derivative (concave upward) rather than the negative second derivative (concave downward) observed in the original data (compare Fig. 2I, top, with Fig. 2F, top). Furthermore, while the reconstructed normalised decision time for correct trials closely matched that of the ground-truth model, for error trials, the normalised decision time was substantially shorter across all evidence quality levels,

indicating a consistent underestimation of decision times for error decisions (compare Fig. 2I, bottom, with Fig. 2F, bottom). These results highlight the inconsistencies introduced by DCM's estimation procedure, potentially unable to make precise estimation to elucidate decision-making mechanisms.

3.3. Cortical columnar model with period-doubling dynamics

To further investigate DCM's ability to infer multistable dynamics, we analysed a cortical model exhibiting period-doubling behaviour. The model space consisted of three candidate architectures: the ground-truth model with lateral connections, an alternative model with only feedback connections, and a fully connected model that includes both lateral and feedback connections (Fig. 3A-C). We trained DCMs using 400 simulated trials for each model in the model space.

In the ground-truth model, the simulated neural activity in column 1 (Fig. 3D, dark grey) exhibited characteristic period-doubling oscillations, where the system alternated between two stable oscillatory states. This behaviour was further reflected in the phase-space trajectory of the ground-truth model (Fig. 3E, dark grey), which showed a structured yet nonlinear pattern indicative of a system transitioning between distinct oscillatory regimes. This was further supported by its Lyapunov exponent value of 0.27.

3.4. DCM correctly identifies period-doubling model architecture but not connectivity strengths

BMS results (Fig. 3F) indicate that the ground-truth model is correctly identified as the most probable architecture. However, despite correctly selecting the model structure, DCM struggles to accurately recover the underlying connection strengths. Specifically,

the inferred lateral connection strengths deviated substantially from those in the ground-truth model, suggesting that DCM did not precisely capture the intrinsic network dynamics governing period-doubling of the original cortical columnar model.

To assess the impact of these estimation errors, we simulated the network using the DCM-estimated connection strengths. The resulting neural activity timecourse (Fig. 3D, blue) deviated from the expected period-doubling behaviour. This suggests that the errors in the estimated connectivity disrupted the fine balance required for multistable oscillatory regimes. Similarly, the phase-space trajectory reconstructed using DCM-estimated connections (Fig. 3E, blue) lacked the well-defined structure of the ground-truth model, instead showing a trajectory indicative of a single stable oscillation, with Lyapunov exponent of zero.

Furthermore, during DCM training, we observed that if the sampling frequency was not sufficiently high, the estimation approach failed to capture the actual oscillatory frequencies of the regime (Fig. S2). This suggests that studies using actual brain data should ensure high sampling rates to properly capture possible multistable regimes in neural activity.

These results highlight a critical limitation of DCM in estimating effective connectivity in networks exhibiting period-doubling. Similar to the decision-making case, while BMS can successfully identify the correct model architecture, inaccuracies in connection strength estimation compromise the ability of DCM to faithfully reconstruct the underlying oscillatory dynamics.

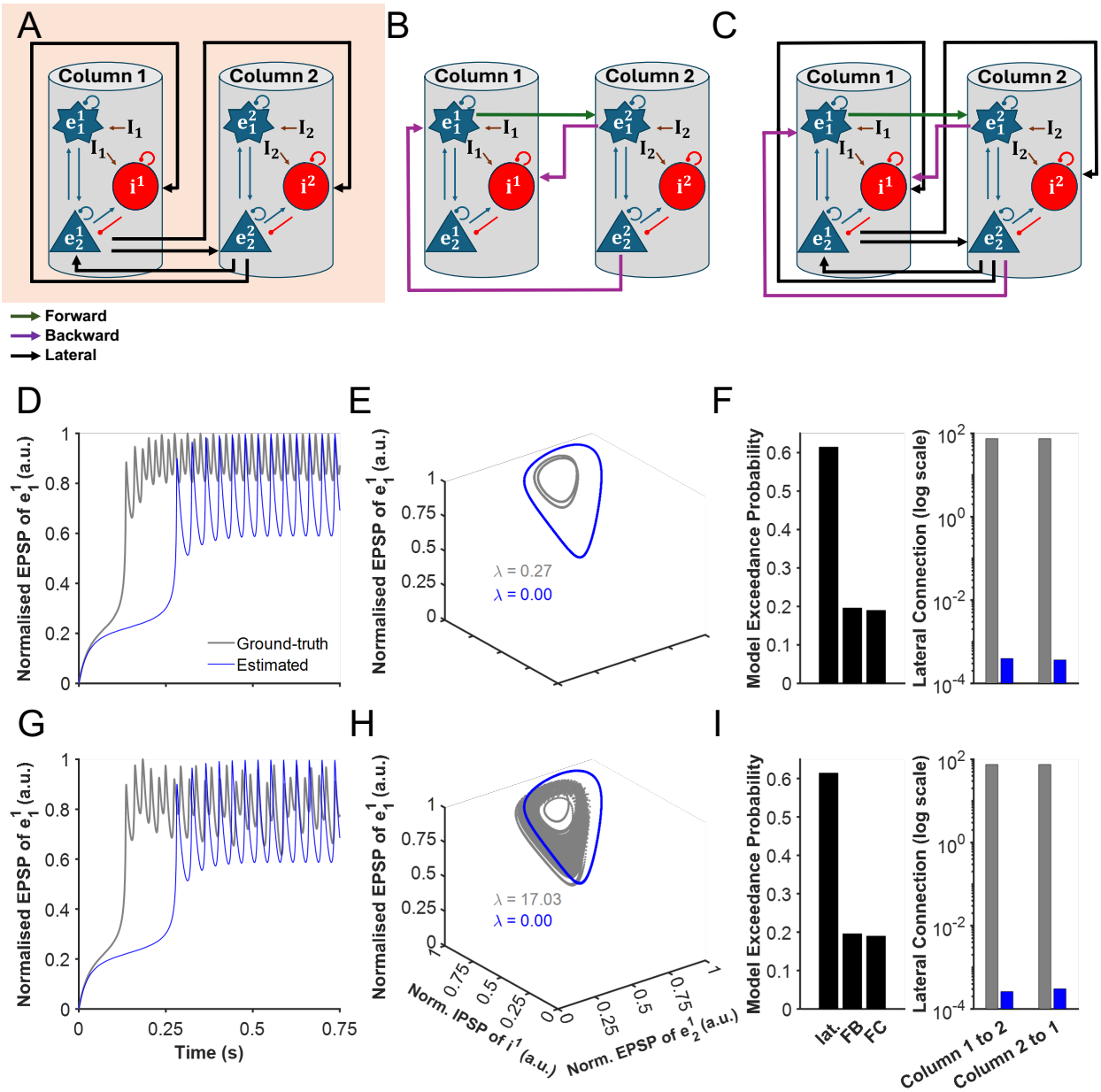

Fig. 3. DCM estimation of period-doubling and chaotic dynamics. (A–C) Same as Fig. 2A-C. (D) Simulated neural activity of e_1 in column 1 for the period-doubling regime, comparing the ground-truth model with the DCM-estimated model. (E) Phase-space trajectories for ground-truth and DCM-estimated (F) BMS results for period-doubling (left), alongside the recovered lateral connection strengths for ground-truth and DCM-estimated (right). G–I: Mirror (D–F) but for chaotic dynamics.

3.5. Cortical columnar model with chaotic dynamics

To investigate DCM's ability to infer a continuum of stable dynamics, we analysed a cortical columnar model exhibiting deterministic chaos. The model space is the same as period-doubling (Fig. 3A-C). Unlike previous cases, the ground-truth model's lateral connections to excitatory and inhibitory populations differ, which plays a critical role in generating the chaotic dynamics observed in this regime. As in previous case, we trained DCMs using 400 simulated trials for each model in the model space.

In the ground-truth model, the simulated neural activity timecourse in column 1 (Fig. 3G, dark grey) exhibited chaotic fluctuations characterised by aperiodic oscillations. This behaviour was further reflected in the phase-space trajectory (Fig. 3H, dark grey), which formed a finite, complex and non-repetitive structure, indicative of a high-dimensional chaotic attractor dynamics with a high Lyapunov exponent value of 17.03.

3.6. DCM correctly identifies chaotic model architecture but not connectivity strengths

BMS results (Fig. 3I) indicate that the ground-truth model was correctly identified as the most probable architecture. However, similar to the previous cases, DCM struggled to accurately recover the underlying connection strengths. The inferred lateral connection strengths deviated substantially from those in the ground-truth model, suggesting that DCM did not effectively capture the nonlinear and highly sensitive interactions characteristic of chaotic dynamics.

To assess the impact of these estimation errors, we simulated the network using the DCM-estimated connection strengths. The resulting neural activity timecourse (Fig. 3G, blue) exhibited a qualitative shift, where chaotic fluctuations were replaced by oscillatory

patterns that lacked the irregularity seen in the ground-truth model. This suggests that the errors in the estimated connectivity disrupted the delicate balance necessary for generating chaotic dynamics. Further, the phase-space trajectory reconstructed using DCM-estimated connections (Fig. 3H, blue) failed to reproduce the complex attractor structure of the ground-truth model, but instead exhibited a single stable oscillatory trajectory with a Lyapunov exponent value of zero. Moreover, similar to the period-doubling case, we found that DCM estimation was highly sensitive to the sampling frequency used during training (Fig. S2). Hence, these results reinforce the limitations of DCM in estimating effective connectivity for multistable neural states.

4. Discussion

In this study, we evaluated the ability of DCM to infer effective connectivity in neural circuits exhibiting multistable dynamics. Using simulated local field potentials of cortical column models as ground truths, we investigated DCM's performance in three cases of neural dynamics: bistable fixed points with decision-making, period doubling with two oscillatory frequencies co-existing, and deterministic chaos. Our results demonstrate that while BMS in DCM reliably identifies the correct model architecture across all cases, DCM struggles to accurately estimate extrinsic connection strengths. In this study, we purposely used local field potential source activity to avoid factors arising from volume conduction and delays (Sanchez Bornot et al., 2018), but DCM still struggles even with such case.

For the bistable decision-making case, we found that DCM-estimated connectivity strengths introduced systematic biases, affecting both decision accuracy and decision

time. Similarly, in the period-doubling and chaotic cases, the estimated connectivity strengths failed to identify the network dynamics, leading to deviations from the network models' activity timecourses, state-space trajectories and Lyapunov exponents from that of corresponding ground-truth models.

Effective connectivity models are often used to infer directed interactions between brain regions (Friston, 2011), and small errors in connectivity strength estimation can lead to incorrect conclusions about neural communication and information processing. Prior research has highlighted certain limitations of DCM, including its tendency to favour more complex models even when a simpler ground truth exists (Litvak et al., 2019), as well as difficulties in estimating synaptic gain which may result in Hopf bifurcations (Moran et al., 2013). Adding to previous findings, our results suggest that DCM's estimation biases can lead to distorted behavioural outcomes. These findings suggest that DCM may not be fully reliable when applied to real-world neuroimaging data where multistability plays a central role, such as in processing decision-making (Wong and Wang, 2006), working memory (Lundqvist et al., 2018), cognitive flexibility (Loh and Deco, 2005), perceptual switching (Rankin et al., 2014), and pathological brain states like epilepsy (Kalitzin et al., 2019).

Our results additionally demonstrate that DCM's ability to estimate connectivity strengths in multistable cortical circuits is highly sensitive to the temporal resolution of the data. Specifically, we observed that when the sampling frequency was not sufficiently high, DCM failed to accurately track the actual oscillatory dynamics of the studied system. This sensitivity is a critical factor for studies applying DCM to real neuroimaging data, particularly in modalities such as EEG and MEG, where sampling rates can vary widely.

Given that previous work has shown that DCM already faces challenges in capturing fast frequency components in neural signals (Friston et al., 2019), our findings reinforce the need for careful consideration of data resolution when using DCM for effective connectivity analysis. Addressing these challenges will require methodological refinements to DCM as well as the exploration of alternative or hybrid approaches that improve its capacity to capture multistable neural dynamics.

To improve DCM's applicability to multistable neural systems, refinements in prior assumptions and model structure are necessary. One approach is utilising adaptive temporal filtering (Arnold et al., 1998) to better capture rapid neural state transitions. Moreover, the current reliance on the Laplace approximation assumes a Gaussian posterior, which may not adequately capture global nonlinear dependencies in complex systems (Chumbley et al., 2007). Using non-Gaussian priors or more flexible variational inference methods (e.g., Khan et al. (2013)) could enhance accuracy in estimating connection strengths. A stronger foundation for bifurcation-aware modelling could be achieved by incorporating dynamical priors that track bifurcations (e.g., Moran et al. (2011)) or machine-learning-based system identification (Wang et al., 2018). These improvements would help DCM better recover multistable dynamics.

While refining DCM could enhance its ability to capture multistable neural dynamics, alternative approaches may offer complementary solutions. Granger causality (Granger, 1969) provides an exploratory method but is limited to linear interactions and is prone to detecting spurious connections, making it less effective for capturing complex cortical dynamics (Asadpour and Wong-Lin, 2024). Data-driven techniques such as recurrent neural networks (Downey et al., 2017) offer flexibility in identifying latent neural states but

lack the interpretability of DCM's structured parameter space. A promising direction is hybrid approaches that integrate DCM with data-driven inference, such as using variational autoencoders (Yang et al., 2023), dynamical systems based regression (Lenfesty et al., 2025), or Bayesian neural networks (Neil et al., 2007) to refine priors, improving estimation accuracy while preserving interpretability.

Taken together, we have evaluated the ability of DCM to infer effective connectivity in neural circuits exhibiting multistable dynamics. While BMS reliably identified the correct model architecture, DCM struggles to accurately estimate extrinsic connection strengths, leading to deviations in simulated neural activity across decision-making, period-doubling, and chaotic regimes. These limitations suggest that while DCM remains a valuable tool for model selection, its application to multistable neural systems should be approached with caution. Future work should focus on refining DCM's parameter estimation methods, incorporating bifurcation-aware modelling, and integrating data-driven approaches to improve its accuracy in capturing complex neural dynamics.

CRediT authorship contribution statement

Abdoreza Asadpour: Conceptualization, Formal analysis, Validation, Visualization, Investigation, Methodology, Writing – original draft, Writing – review & editing. **Amin Azimi:** Formal analysis, Validation, Visualization, Methodology, Investigation, Writing – original draft, Writing – review & editing. **KongFatt Wong-Lin:** Conceptualization, Validation, Supervision, Project administration, Funding acquisition, Writing – original draft, Writing – review & editing.

Code and data availability

The source code for our implementation and generated data are available upon publication.

Declaration of competing interest

The authors declare no competing interests.

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