Egocentric body-axis-related and allocentric clover-like tuning of object vector representations supports human spatial cognition

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1 Abstract

Vector-based spatial representation is key for navigation, mapping direction and distance between self and environment. Though observed in rodents, its neural basis in humans remains unclear. Using high-resolution imaging and a novel spatial updating task, we found vectorial representations in retrosplenial and parahippocampal cortex, extending to parietal and entorhinal areas in self- and object-centered coordinates, respectively. Egocentric directional signals peaked when the object was behind the navigator, while distance signals emerged only when the object was out of view, suggesting these signals might act as mnemonic buffers for vision-independent spatial mapping. Allocentric directional signals

formed a clover-shaped four-axis pattern aligned to a common visual feature, with improved

navigation accuracy along these axes, highlighting their functional relevance for human nav-

igation. Rodent parallel single unit recordings indicated the clover pattern resulted from the

average activity of neurons with allocentric vectorial properties, suggesting a shared, cross-

species mechanism. Collectively, our findings demonstrate a vector-based population code

detectable via fMRI, potentially serving as a neural reference axis that anchors objects to

internal maps, supporting flexible navigation and perhaps broader cognition.

2   Introduction

Vectorial representation of space provides a powerful navigation tool because it allows

mapping of geometric relationships (direction and distance) between the self and the external

world (objects or boundaries) through self-motion[9]. Combined with self location representa-

tion (place cells)[40], path integration (grid cells)[25] and heading representation (head-direction

cells)[54], object- and boundary-vector codes[29,2,35,13,46,58] represent the presence of a salient

cue at specific locations relative to an agent, even when the cue is not directly in sight, while

theoretically allowing for vector arithmetic and vectorial definition of a goal location.

Vector-based codes have been described in the rodent brain in egocentric (self-centered)

frame of reference (eg. in parietal cortex [PC], retrosplenial cortex [RSC], postrhinal cortex

[POR] (rodent homologue of the parahippocampal cortex, [PHC]) and striatum [STM])[2,28,21]

and in allocentric frame of reference (eg. in entorhinal cortex [EC], subiculum and hippocam-

pus [HP])[35,13,29]. These observations are generally in line with a theoretical model whereby

egocentric representations (in PC) are transformed into allocentric ones (in the medial tempo-

ral lobes) by head-direction modulated representations in the RSC[8]. Overall in rodents and

humans, the vectorial response to boundaries and their prominent role for navigation and be-
yond has been well studied[15,16,7,55,56], whereas evidence concerning object-related vectorial
response are scarcer in rodents, and entirely lacking in humans.

If all distances and directions were equally represented in the brain, it would theoreti-
cally be impossible to detect any macroscopic vectorial signal in the human brain using func-
tional magnetic resonance imaging (fMRI)[39]. However, evidence shows that vector-sensitive
receptive fields cover space non-uniformly: for instance, populations of egocentric boundary
cells in RSC show a preferential tuning to short distance ranges and directions behind the
animal[2], while populations of allocentric object-vector cells in medial EC (rodent homologue
of the posterior-medial entorhinal cortex [pmEC]) show sparser representations of farther
distances from an object[29].

Based on this assumption, the current study aimed at identifying object-related al-
locentric/egocentric direction and distance modulation in the human brain using a spatial
updating task, where participants have to point back at an intramaze object after periods
of self-motion. Based on the above rodent studies and studies in humans[51,10], the locations
expected to represent distance and direction to an object include the PC, RSC, PHC, EC and
HP. We also sought to characterize the neural population tuning response in relation to an
object distance/direction, and verify the functional relevance of those codes for human spatial
orientation and navigation.

3   Results

3.1   Mapping directional and distance tuning during spatial navigation.

Here, we used 7T fMRI to monitor the brain activity of 47 young participants navigating a virtual arena surrounded by distal landmarks (a mountain scenery and a castle) and with a large object (a column) situated in the northeast quadrant (fig. 1a-c). During the task, participants alternate between actively navigating to start locations scattered around the object and being passively transported along predefined trajectories. Throughout the passive transportation the object is invisible, but participants must keep track of its location and point back to it (fig. 1d-h). The current object vector experienced from a given start location is updated by self-motion (experienced while being passively moved along a given trajectory) in order to be able to accurately point back at the object at the end of the trajectory. Start and end locations of the trajectories were rigorously controlled in order to ensure full coverage of all directions and distances to the intramaze object, see Methods. Responses occurred either from an egocentric perspective (i.e. egocentric condition: "the object is ahead/behind/left/right of me at the end of the trajectory") or from an allocentric perspective (i.e. allocentric condition: "I am North/East/South/West of the object at the end of the trajectory"). While both egocentric and allocentric representations theoretically coexist during spatial navigation, the two conditions and trajectories were designed to provide a behavioral readout of spatial updating performance at different directions and distances to the object and along the two frames of reference (allocentric and egocentric). Two categories of fMRI models were estimated: 1) parametric modulation analyses were used as 'localization' models to identify voxels in the brain which activity varied with *(i)* the egocentric direction to the

object, *(ii)* the allocentric direction to the object and *(iii)* the distance to the object, whereas

2) tuning models discretized the data into evenly-spaced bins in order to characterize the

BOLD response variation to changing self-object relationships (see 6.1.7 for model specifics).

Group-level peak activity in the parametric modulation models served as *a priori* locations

for the tuning model's estimation.

3.2 Spatial updating performance and gaze pattern during the task.

Pointing error in the allocentric condition was slightly higher than the egocentric con-

dition ($F_{(46,1)}$=7.07, p=0.011, generalized eta-squared (ges): η^2_g=0.027, fig. 2a-b). Two-way

ANOVAs show a significant effect of the direction at which the trajectory lies in both the ego-

centric condition (direction: $F_{(1.71,68.45)}$=16.002, p<0.0001, η^2_g=0.066, distance: $F_{(2,80)}$=0.09,

p=0.9, η^2_g=0.0002, interaction: $F_{(4,160)}$=0.36, p=0.8, η^2_g=0.002) and allocentric condition (di-

rection: $F_{(2,78)}$=24.19, p<0.0001, η^2_g=0.094, distance: $F_{(2,78)}$=2.14, p=0.12, η^2_g=0.006, inter-

action:F(4, 156)=1.54, p=0.19, η^2_g=0.008, fig. 2c), with trajectories going towards the object

associated with worst pointing performance. This analysis was performed for n=41/40 since

there were missing observations in 6/7 participants in the egocentric or allocentric condition,

respectively.

To understand which cues participants used during the task, we estimated gaze dwell

times during the orientation phase, where participants had unlimited time to look around

and to orient at the start location. We separated dwells to three areas of interest in the

environment: the background (where distal landmarks are), the object and the ground (fig.

2d). We found that participants spent significantly more time looking at the distal land-

marks (Wilcoxon signed-rank W=54, p<0.0001, r=-0.74), particularly at the northern-most

Figure 1. Spatial navigation task in virtual reality (VR) (a) Isometric view of the circular wall-free arena with an intramaze object (i.e. the column); (b) The arena is surrounded by distal landmarks, projected at infinity; (c) First-person view of the environment with the intramaze object and the main distal landmark (i.e. castle) situated in the North; (d) The task alternates between periods of active (dashed lines) and passive (thick lines) navigation, scattered around the object (black dot) to ensure full direction and distance coverage. (e-h) A trial starts with an active *navigation* phase to a start location, where participants get unlimited time to *orient* themselves and look around. Upon key press, the object disappears and participants are passively moved along a predefined *trajectory*, during which they have to maintain the position of the now invisible object in mind. At the end location, participants have to point back to the object, giving their *response* from either an egocentric perspective ("the object is ahead/behind/left/right of me", as depicted in g) or an allocentric one ("I am North/East/South/West of the object", as shown in h). Responses are recorded as a continuous variable (in degrees). *Feedback* is provided according to performance.

Figure 2. Behavioural spatial updating results. Mean error in degrees: (a) accumulated across all blocks and participants, (b) along the 10 blocks of egocentric (red) and allocentric (purple) trials and (c) across different distances and egocentric directions to the object. (d) Proportion of time spent looking at 3 areas of interests (the background, the object, the ground) during the orientation phase of the experiment, separately for the two conditions. (e) Gaze heatmaps during the orientation phase of egocentric and allocentric condition, respectively. Gaze intersections on the object were removed from the heatmaps for visualization purposes. Heatmaps were normalized collectively across the two conditions.

landmark (the castle, see. fig. 2e) in the allocentric condition compared to the egocentric condition while the time spent looking at the object (the column) was similar in both conditions (W=415, p=0.34, r=0.16). In contrast, participants spent more time looking at the ground, close to the object location (fig. 2e) during the egocentric condition (W=568, p=0.0002, r=0.60).

3.3 Body-axis directional tuning of egocentric object vector representations.

We first estimated the localization model with a parametric modulation analysis where direction to the column was mapped to the interval [-1,1], where -1 corresponds to the object behind and 1 to the object in front of the participant. We identified three key effects in our regions of interest: a positive modulation in posterior parietal cortex (coordinates: [48,-50,44], Brodmann area 39), and negative modulations in both retrosplenial cortex (coordinates: [20,-51,8], Brodmann area 23) and parahippocampal cortex (coordinates: [21,-42,-8], Brodmann area 36) (fig. 3a). To better understand how the activity varied with changing self-object relationships, we further discretized the observed egocentric directions into 8 evenly-spaced bins (tuning model specified in 3b-c). Here, we found higher signal in PPC when the object was straight ahead of the participant, while in RSC and PHC, activity peaked when the object was behind the participants (bins 1 and 8) (fig. 3d-g).

A one-way ANOVA with egocentric direction bins as a within factor showed a significant omnibus effect in the three ROIs: PPC ($F_{(5.64,208.65)}$=8.65, p<0.001, η_g^2=0.093), RSC ($F_{(4.51,175.91)}$=35.21, p<0.001, η_g^2=0.25) and PHC ($F_{(4.66,172.57)}$=44.44 , p<0.0001, η_g^2= 0.30). Post-hoc polynomial contrast showed a significant quadratic and, to a lesser extent, quartic tendencies in the three ROIs: in PPC (linear: $t_{(37)}$=-0.27, p=0.79; quadratic: $t_{(37)}$=-7, p<.0001; cubic: $t_{(37)}$=1.09, p=0.28; quartic: $t_{(37)}$=3.13, p=0.003; 9 outliers removed), RSC (linear: $t_{(39)}$=2.25, p=0.03, does not survive Bonferroni correction; quadratic: $t_{(39)}$=11.81 , p<0.0001; cubic: $t_{(39)}$=-0.37 , p=0.71; quartic: $t_{(39)}$=-3.53, p=0.001; 7 outliers removed) and PHC (linear: $t_{(37)}$=2.49, p=0.01, does not survive Bonferroni correction; quadratic: $t_{(1,37)}$=11.83, p<.0001; cubic: $t_{(37)}$=0.91, p=0.36; quartic: $t_{(37)}$=-7.04 , p<.0001; 9 outliers removed).

To better understand if egocentric direction modulation gave any advantage to naviga-

tion, we correlated the average parametric modulation from the localization model (fig. 3a)

with task performance and two spatial cognitive tests performed at the end of the experiment

(the Perspective taking test and 4 Mountains test, supp. fig. S1). Generally, we found the

error (expressed as a z-score) to be lower, thus performance was better in people showing

the strongest modulation in PPC, but this correlation did not survive multiple comparison

correction (egocentric: r=-0.34, p=0.02; allocentric: r=-0.26, p=0.074, Spearman correlations,

see supp. fig. S1 for the same data in RSC and PHC). No other correlation was significant.

Finally, since rodent data indicate a contralateral bias in representing egocentric vec-

tor to boundaries[2] (that is, left RSC represents contralateral directions and vice-versa), we

tested for hemispheric lateralization with right/leftward object being mapped as 1/-1 (see fig.

3i and caption). We indeed observed two contralateral peaks of activation in RSC, with the

left hemisphere coding for when the object was situated to the right of the subject (coordi-

nates: [-18, -58, 12], Brodmann area 23), and the right hemisphere coding for when the object

was leftward (coordinates: [11, -50, 32], Brodmann area 23). Additional peaks were found

in the left hemisphere (in parietal cortex at coordinates: [-6, -50, 50], Brodmann area 7 and

close to PHC at coordinates [-28, -49, -6], Brodmann area 19).

3.4   Clover-like directional tuning of allocentric object vector representations.

For allocentric directions, we initially mapped North/South directions as 1/-1, and

found 2 clusters of direction-modulated activity in our areas of interest: RSC (coordinates:

[20,-56,13], Brodmann area 23) and PHC (coordinates: [21,-35,-12], Brodmann area 36).

When estimating the tuning models with 8 allocentric direction bins, we discovered that

Figure 3. Egocentric directional modulation of the fMRI signal. (a) Localization model: whole brain effect of voxels showing a positive/negative parametric modulation of activity by egocentric direction in pink/blue, respectively. Three peaks in our regions of interest were identified: posterior parietal cortex (PPC), retrosplenial cortex (RSC), parahippocampal cortex (PHC). Maximum and minimum T-scores are shown together with the slice location in MNI coordinates. FWE=family-wise error correction. (b-c) Egocentric directions (ahead, behind, left, right) were discretized into 8 equidistant bins that were further used to estimate the tuning model in a 2-voxel-radius sphere centered on previously identified peaks. Boxplots in (c) show the number of events for each bin averaged per runs with the median, 25th and 75th percentiles (black box), 1.5 x interquartile range (whiskers), and outliers (dots). (d-f) Median tuning curves in PPC (d), RSC (e) and PHC (f), represented by the average beta estimate in a given sphere for different egocentric directions bins. Shaded areas indicate the between-subject standard error of the mean (s.e.m.). (g) Individual tuning curves in RHC and PHC are shown as best examples. (h) Hemispheric lateralization model: whole brain parametric modulation with positive/rightward object and negative/leftward object modulation in yellow and blue, respectively. On the slice, the left hemisphere appears on the left, following neurological convention.

activity in those areas increased at three or four seemingly orthogonal directions around the

object (bins 2/4/6/8, fig. 4f). This pattern of activity (peaks in bins 2/4/6/8, troughs in bins

1/3/5/7) was observed in most participants (see individual examples on fig. 4h). Based on

this observation, we ran an additional localization model that mapped bins 2/4/6/8 as 1 and

1/3/5/7 as -1 (see pure clover model in section 6.1.7). This model confirmed our clusters in

RSC and PHC (fig. 4a, positive modulation) and identified a third peak in entorhinal cortex

(EC), particularly in the posterior-medial section (pmEC, fig. 4b, negative modulation). When

estimating the tuning model in pmEC (fig. 4c-d), we observed that, contrary to RSC and PHC,

activity in EC was higher in bins 1/3/5/7 (light areas on fig. 4e, left). Nevertheless, the pat-

tern in EC was similar, with the BOLD signal being higher around three or four directions

to the object. One-way ANOVAs with bins as a within factor confirmed a significant omnibus

effect in all three ROIs (RSC: $F_{(3.98,163.28)}$=6.37, p<0.001, η_g^2=0.036; PHC: $F_{(4.53,167.75)}$=4.46,

p<0.001, η_g^2=0.032; EC: $F_{(5.22,177.36)}$=5.13, p=0.025, η_g^2=0.023) and a post-hoc contrast con-

firmed that the activity bins 2/4/6/8 significantly differed from activity in bins 1/3/5/7 (RSC:

$t_{(41)}$=-4.442, p<.0001; 5 outliers removed; PHC: $t_{(37)}$=-4.446, p<.0001; 9 outliers removed; EC:

$t_{(34)}$=2.43, p=0.02; 12 outliers removed).

To better understand this pattern of neural responses, we ran a more detailed tuning

model with 16 bins representing 16 discretized allocentric directions relative to the object

(fig. 4g). The 3/4 peaks in RSC and PHC, although not entirely orthogonal to each other,

formed a clover-like pattern of activity around the object. In reference to the main landmark

situated in the North (between bins 8 and 9 on fig. 4g), the closest peak in directional bin 7

was located 33.75° away from the main North axis defined by the environment.

When correlating the strength of the parametric modulation with task performance,

we found positive correlations whereby stronger clover-like modulation was associated with

being better at pointing back at the object, although statistics did not survive multiple com-

parison correction (see supp. fig. S2 for details). We nevertheless wondered whether pointing

performance would be impacted by the location of the trajectories with respect to the clover

axes, i.e. whether spatial updating for trajectories located on clover axes (dark grey tra-

jectories on fig. 4e, right) would be any better than for trajectories located off clover axes

(light grey trajectories on fig. 4e, right). We found a small but significant effect in which

participants were better at pointing back at the object from an allocentric perspective when

trajectories were situated on rather than off the clover axes (allocentric condition: $t_{(46)}$=-2.69,

p=0.009; egocentric condition: $t_{(46)}$=-1.1, p=0.27, data averaged over bins 1/3/5/7 and 2/4/6/8,

fig. 4j).

3.5 Neurons in rodent retrosplenial cortex exhibit clover-like directional and distance tuning to objects.

We next asked whether the clover-like pattern of activity observed in humans also ex-

isted in the rodent brain, either at the individual cell or population level, and whether this

spatial code was related to cells having vectorial attributes. To do so, we recorded single

units from the rodent retrosplenial cortex (areas 29 and 30, deep layers, fig. 5a and supp.

fig. S3a) during an open field foraging task in a rectangular arena (1.5m*1.5m) with a cue

card on the north wall and a single circular intramaze object in the north-east quadrant (fig.

5b). Analogous to human fMRI data analyses, we used GLM-based forward model selection

to classify cells according to their vectorial allocentric and egocentric attributes (i.e., direc-

tion, distance, and their first derivatives) and combinations thereof (details in Section 6.2).

Figure 4. Allocentric directional modulation of the fMRI signal. (a-b) Localization model: whole brain effect of voxels showing a positive/negative parametric modulation of activity by allocentric direction in pink/blue, respectively. Two peaks were identified in RSC and PHC. An additional peak in posterior-medial EC (pmEC) was identified at an uncorrected threshold of p<0.001 (unc. on b), identified by the arrow. Maximum and minimum T-scores are presented together with the location of the display slice in MNI coordinates. FWE=family-wise error correction. The model estimates shown here correspond to the pure clover model (see sec.6.1.7 for explanation). (c-d) Allocentric directions to the object (North, East, South, West) were discretized into 8 equidistant bins and used to estimate the tuning model in a 2-voxel-radius sphere centered on previously identified peaks. Boxplots in (d) show the number of events for each bin, averaged per run, with the median, 25th and 75th percentiles (black box), 1.5 x interquartile range (whiskers), and outliers (dots). (e) Individual example of navigation (left) and trajectory (right) paths lying on (dark grey: bins 2/4/6/8) or off (light grey: bins 1/3/5/7) clover axes (f) Median tuning curves in RSC, PHC and EC across 8 allocentric directions bins. Shaded areas indicate the between-subject standard error of the mean (s.e.m.). (g) Median tuning curves in RSC and PHC in 16 allocentric direction bins. Outlier data points were removed before calculating the group median. (h) Individual tuning curves in RSC and PHC for the 8 bin model are shown as best examples. Interestingly, the same four peak structure in those brain areas was observed in most participants. (i) Pointing error (in degrees) on and off the clover axes in the egocentric (left) and allocentric (right) conditions. Participants are better at pointing back to the object when the trajectory lies on the clover axes in the allocentric condition. Errors are averaged over bins.

Our analysis revealed that approximately 26% of the 149 single units exhibited allocentric directional and distance tuning (fig. 5c, green bar), which was the most common functional classification among all covariates tested.

    The spatial firing patterns of these neurons showed a notable structure, with individual cells displaying distinct firing fields around the object (fig. 5d), the majority of which exhibited multiple peaks (fig. 5e). The distribution of peak locations was evenly distributed across the population (fig. 5f), with a notable clustering of peaks closer to the object. The population-level analysis revealed a clear clover-like pattern in the median normalized firing rates of cells (fig. 5h), reminiscent of the activity patterns observed in humans. Statistical comparison between the original and shuffled data (fig. 5i) confirmed the significance of this spatial organization (KS statistic = 0.333, p-value = 0.036), with the highest peak located approximately 45° off the north of the arena. By comparison, the same analysis performed on neurons with egocentric tuning properties (distance and direction relative to the animal) did not reach significance (KS statistic = 0.306, p-value = 0.069, see supp. fig. S3b), suggesting that the clover-like pattern was a feature of allocentric vectorial cells in the recordings.

Figure 5. Allocentric vectorial coding in rodent retrosplenial cortex. (a) Schematic representation of recording locations in deep layers of areas 29 (blue) and 30 (pink) in retrosplenial cortex; the probe track is highlighted (red). (b) Experimental setup showing the 1.5×1.5m arena with Northern cue card and circular object (black circle) in the North-East quadrant. Green and blue arrows indicate object-centric and egocentric reference frames, respectively. Animal trajectory during a single recording session, showing complete coverage of the arena. (c) GLM-based classification of neurons showing the percentage of cells explained by different covariates or combinations thereof. Green bar highlights neurons with allocentric directional and distance tuning. d=derivative. Covariates with classified cells count lower than 2 are not shown on the figure. (d) Firing rate maps of four individual neurons displaying object vectorial properties. (e) Distribution of the number of firing rate peaks among neurons in the population. (f) Polar plot showing the distribution of peak locations (angle and distance, in cm) for all detected peaks across the population, with the object at the plot origin. Each dot represents a single peak. (g) Population analysis showing the median normalized firing rate across all neurons with allocentric vectorial properties. Green line indicates the median, and shaded area represents SEM. (h) Firing rate comparison between the original (green line) and shuffled (dashed line) distribution. Left: firing rate across angles relative to the object. Right: cumulative probability distributions of firing rate differences between original and shuffled data relative to the mean firing rate for the session. KS= one-sided Kolmogorov-Smirnov test.

3.6 Mnemonic rather than perceptual distance tuning of allocentric object vector representations in humans.

To estimate distance modulation on the human brain data, we normalized distance data with minimum/maximum distance as 1/-1. We found four peaks in our areas of interest: in RSC (coordinates: [-18,-59,12], negative modulation with increasing activity for increasing distance, Brodmann area 23), PHC (coordinates: [18,-35,-14], negative modulation, Brodmann area 36), EC (coordinates: [-24,5,-38], positive modulation) and HP (coordinates: [-22,-11,-12], positive modulation, fig. 6a). The two medial temporal peaks were observed at uncorrected whole brain threshold only. We then discretized this data into 8 equidistant bins (fig. 6b), but due to the nature of the task (start and end points of the trajectories are scattered around the object), middle bins corresponding to medium distance were observed more often than extreme bins, corresponding to very small or very large distances, leading to an unbalanced model (fig. 6c). When estimating this model, we found a significant omnibus effect for the distance bins in RSC ($F_{(2.95,94.40)}$=5.56 , p=0.002, η_g^2=0.09) and PHC ($F_{(2.84,85.28)}$=2.95, p=0.04, η_g^2=0.065), but no effect in EC ($F_{(3.13,81.32)}$=1.62, p=0.19, η_g^2=0.036) or HP ($F_{(3.82,76.48)}$=1.10, p=0.36, η_g^2=0.03). Proceeding with polynomial post-hoc contrasts we found a significant linear trend both in RSC (linear: $t_{(32)}$=5.81, p<.0001; quadratic: $t_{(32)}$=-0.75, p=0.45; cubic: $t_{(32)}$=1.73, p=0.09; quartic:$F_{(32)}$=-0.96, p=0.34; 14 outliers removed) and PHC (linear: $t_{(30)}$=4.39, p=0.0001; quadratic: $t_{(30)}$=-1.45, p=0.15; cubic: $t_{(30)}$=1.31, p=0.19; quartic: $t_{(30)}$=-0.20, p=0.83; 16 outliers removed), indicating a linear relation between distance and neural activity in those two clusters (fig. 6d, see also individual examples in fig. 6f).

Based on the observation that the between- (fig. 6d) and within-subject (fig. 6f) vari-
ance in beta estimates was particularly high when participants came closer to the object
(bins 1 and 2), we reasoned that those two areas could be sensitive to fast-changing visual
inputs. We thus decided to rerun the model separating moments in time where the object
was visible or invisible, and assess whether the distance modulation held. We found that
RSC and PHC activity scaled up with increasing distance only when the object was invisible
(fig. 6g). We confirmed this observation with our tuning model (fig. 6e), which accounted
for the fact that these models were estimated on roughly half the amount data since the the
number of distance bins was reduced to 4 (see sec.6.1.7). Both areas indeed seemed to react
to the immediate vicinity of the object, as the beta estimate in bin 1 significantly differed
from the rest of the bins in the visible model (posthoc contrast: RSC: $t_{(29)}$=-4.14, p=0.0003,
17 outliers removed; PHC: $t_{(39)}$=-2.88, p=0.006, 7 outliers removed). However, past bin 1,
RSC and PHC still coded for distance when the object was out of sight (invisible model in
RSC: linear: $t_{(40)}$=8.72, p<.0001, quadratic: $t_{(40)}$=2.71, p=0.02, does survive Bonferroni cor-
rection, 6 outliers removed; invisible model in PHC: linear: $t_{(39)}$=9.52, p<.0001, quadratic:
$t_{(39)}$=3.48, p=0.0025, 7 outliers removed) but not when the object was visible (visible model
in RSC: linear: $t_{(29)}$=0.67, p=1, quadratic: $t_{(29)}$=0.79, p=0.87, 17 outliers removed, visible
model in PHC: linear: $t_{(39)}$=1.01, p=0.63, quadratic: $t_{(39)}$=0.58, p=1, 7 outliers removed). No
significant association was found between distance modulation and task performance.

Figure 6. Distance modulation. (a) Localization model: whole brain parametric modulation with positive/negative modulation in pink/blue, respectively. Four peaks were identified: retrosplenial cortex (RSC), parahippocampal cortex (PHC), entorhinal cortex (EC, rather in the anterior portion) and hippocampus (HP). Maximum and minimum T-scores are presented, together with the displayed slice location, in MNI coordinates. FWE=family-wise error correction. The EC and HP peaks were observed at uncorrected threshold only (unc.). (b-c) All distances to the object were used to estimate the tuning model. Boxplots in (c) show the number of events for each bin, averaged per runs with the median, 25th and 75th percentiles (black box), 1.5 x interquartile range (whiskers), and outliers (dots). Note that this model has extremely unbalanced observations. (d) Median tuning curves in RSC and PHC, represented by the average beta estimate in the sphere of interest. Shaded areas indicate the between-subject standard error of the mean (s.e.m.). EC and HP ROIs were not estimated with this model since the omnibus effect in these clusters was not significant (see text). (e) Median tuning curves in RSC and PHC in more parsimonious models with only 4 distance bins, when the object was directly visible (yellow curves) or not (blue curves). (f) Individual tuning curves for the 8 bin model are shown as best examples. (g) Whole brain parametric modulation with distance, for time points where the object is visible (yellow) and invisible (blue). Both negative and positive modulations are aggregated on the map.

3.7   Topographical gradients of ego- and allocentric direction and distance modulation.

Beyond examining peak location and tuning curves within our fMRI regions of interest, we next aimed to describe more specifically the anatomical topography of those responses. To do so, we averaged the parametric modulation maps across participants (fig. 7a-i). The pattern in RSC for the egocentric direction model, although peaking in Brodmann area (BA) 23, extended medially and ventrally within the RSC complex to BA 29 and 30 (fig. 7a-c), whereas the allocentric direction and distance models both yielded higher activation in the dorsal-lateral RSC, near BA 23 and 31. Regarding PHC, stronger modulation was observed in the posterior-medial portion of the ROI, with no clear difference between the three models. In EC, the allocentric direction modulation mapped posterior-medially, corresponding to the pmEC subregion. Finally, HP and EC showed signs of distance modulation in the anterior sections of both regions.

Figure 7. Topographical gradients of ego- and allocentric direction and distance modulation in retrosplenial, parahippocampal and entorhinal cortices and hippocampus. Each map displays the parametric modulation for each voxel in the ROIs, averaged across participants. 3D locations are expressed as voxel indices, with the anterior-posterior (A-P) axis shown on each panel. Color bars are normalized by the minimum and maximum values within a bilateral ROI. Additionally, a transparency map was added to the color map, with higher transparency values for parametric modulation values closer to zero.

4 Discussion

This study investigated how the brain processes vectorial information relative to an intramaze object. We found evidence for distance, as well as ego- and allocentric directional modulation of brain activity as participants navigated around the object. Egocentric directional tuning was observed in posterior parietal, retrosplenial, and parahippocampal cortices with BOLD activity peaking when the object was exactly behind the participant. Allocentric tuning was observed in retrosplenial, parahippocampal, and entorhinal cortex, where brain activity clustered around four allocentric directions, forming a clover-like pattern. In vivo electrophysiological recordings revealed a similar four peak pattern of activity in the rat retrosplenial cortex, suggesting that allocentric vectorial cells may contribute to this specific clover pattern. In humans, the concurrent spatial updating task provided behavioral readouts of participants' ability to track the object while moving around the environment. We found that the strength of allocentric updating was more accurate along the clover axes, highlighting the importance of both types of directional modulation for navigation. Finally, distance tuning was observed in the retrosplenial and parahippocampal cortex in humans, but only when the object was not directly in sight.

Brain activity clustered around four allocentric directions to the object, forming a clover-like pattern in the retrosplenial cortex (RSC), parahippocampal cortex (PHC), and entorhinal cortex (EC). The predominant direction was tilted away from the main landmark in the arena's arbitrary North. Participants with stronger allocentric modulation, particularly in the PHC, performed better on the task, suggesting that this clover-like signal provides a navigational advantage. Coherently, allocentric task performance was also better along the

clover axes. Electrophysiological recordings in rat retrosplenial cortex confirmed a similar

four-fold pattern relative to an object, likely due to the average activity of neurons with ob-

ject vectorial properties. The clover axes in rodents were also tilted away from the Northern

cue card. Besides confirming our human data, to our knowledge this is also the first demon-

stration of allocentric vectorial neurons in the rodent retrosplenial cortex. While it is unclear

how the neurons described in retrosplenial cortex relates to previously observed object-vector

cells in the entorhinal cortex[29], we suggest further studies are needed to characterize the ex-

tent of allocentric and egocentric vectorial representation in the rodent brain. Our human

study could provide a translational basis for informing future targeted studies in rodents.

What is the possible origin and nature of this clover-like pattern? First, we do not be-

lieve that the clover pattern is simply a reflection of the environmental layout, as was the case

for travel axis-tuned neurons in subiculum[41] or multidirectional head direction cells in retro-

splenial cortex[60], where bidirectional or quadridirectional firing was controlled by boundary

arrangements or compartment symmetries, and disappeared in an open arena. Similarly in

humans, the six-fold symmetry generally observed in the entorhinal cortex[14] can be trans-

formed into a four-fold symmetry by local barriers, interpreted as a compartmentalization of

grid-like representations[26]. The fact that the clover was observed in environments with sim-

ple square walls (rodent experiment) or no walls at all (human experiment) points towards

an independence from boundary layout. The common denominator between the human and

rodent experiments thus is the presence of the proximal object within an open field. Sec-

ond, we do not believe the clover pattern reflects landmark structure, as the arena used

for humans contained multiple distal landmarks whose arrangements did not match the

clover axes alignment. However, the consistent alignment of the clover axes among different

human participants indicated that the clover pattern anchored to distal landmarks, likely

the most salient one accessible. The underlying principle organizing the anchoring of the

clover axes ($33.75°$ from the main landmark in humans or $45°$ from the cue card in rodent)

needs further investigation. Third, our data indicate that the presence of the clover-like

pattern is task-independent, as it was observed in complex tasks in humans and a simple

free foraging tasks in rodents. This suggests the clover would be present at all times to

inform and support object-related representations. The direct link to spatial cognition is

demonstrated by improved allocentric spatial updating when participants navigated along

the clover axes, underscoring the behavioral significance of this clover-like signal for nav-

igation. Further research is needed to understand how these object-based representations

interact with boundary-based representations to facilitate goal-directed behavior, as seen

in EC[51,10]. Our spatial task focused solely on a unique object, making it challenging to

distinguish between object and goal-oriented representations. Fourth, the role of object- or

boundary-vector cells is to map the presence of spatial cues of interest, and it is theoretically

beneficial for the mapping of distance/direction to be evenly distributed through space. The

clover pattern could thus represent an additional population code, akin to a neural refer-

ence axis that anchors object representations. Collectively, our results support the idea that

the four peak structure is a reflection of vectorial codes in the brain and is expressed in a

population code that the summative nature of the BOLD signal is able to detect.

We observed that brain activity varied based on the egocentric direction to an ob-

ject, following a quadratic shape, with the highest activity in retrosplenial cortex (RSC) and

parahippocampal cortex (PHC) when the object was positioned behind the participant. This

suggests that these areas may compensate for the lack of direct visual perception to maintain

object direction representation. The strength of this quadratic modulation in the posterior parietal cortex (PPC) was reversed (higher beta weights when the object is in front) and linked to better performance in pointing back to the object from an egocentric perspective. Interestingly, RSC activity showed contralateral bias, with the left and right hemispheres representing contralateral object directions, consistent with previous findings in rodents[2].

Finally, distance modulation was observed in human RSC and PHC. Activity in those brain areas was strongly influenced by the immediate vicinity of the object, and our control analysis indicated that PHC and RSC appeared to code for distance only when the object was not in sight. It is possible that visual inputs solely (e.g. monocular and binocular depth perception, or motion parallax) are sufficient to estimate distance to the object when it is visible[50]. This information processed in the visual cortex might inhibit or saturate activity in RSC/PHC, which then would act as memory buffers to maintain the representation of the object when it cannot be perceived directly. It is an exciting possibility that the mnemonic nature of this distance code could extend beyond spatial navigation to more abstract cognitive processes such as episodic memory or time perception.

5   Conclusion

In summary, by using neuroimaging in humans and electrophysiology in rodents in parallel, our study uncovered and characterized novel types of vectorial (distance and direction) representations in the mammalian brain. Our data contribute to recent work describing vector-encoding neurons that map geometric relationships between the agent and proximal objects[9,2,29,58,5]. We believe these vectorial brain mechanisms complement spatial codes for location[43], path integration[25] and heading[54] to permit flexible navigation, while being par-

ticularly advantageous when environments lack natural boundaries but contain proximal objects. It remains to be determined if and how these egocentric and allocentric spatial codes are used as a basis for vector-based, goal-oriented navigation and possibly cognition beyond space more generally.

6   Methods

6.1   Human experiments

6.1.1   Participants. 57 participants are enrolled in this study. Four participants are excluded due to nausea and six participants are excluded due to experimental error or scanner issue, leading to a final sample size of 47 (range: 18-34 years, μ=25.6, σ=4.12, 20 females, 27 males). All experimental procedures are performed in accordance with the tenets of the Declaration of Helsinki, and are approved by the Norwegian Regional Committee for Medical and Health Research Ethics (REK Midt, 17.02.2021–220248). All participation is voluntary. Potential participants are recruited by word of mouth or posters at the University and Hospital campuses. All participants give informed consent approval. 14 participants out of 47 are invited a second time to perform a control experiment (see section 6.1.2). Participants receive a financial compensation of 120 NOK (~12 euros) per hour.

Inclusion criteria for this study are: (i) healthy, competent volunteers between the ages of 18 to 35, (ii) normal or corrected-to-normal vision, (iii) normal, uncorrected hearing, (iv) English fluency. Exclusion criteria are: (i) ongoing neurological or psychiatric treatment, (ii) history of brain injury, surgery or epilepsy, (iii) work in the metal-processing industry, (iv) pregnancy, (v) presence of foreign objects in the body, such as pacemaker, defibrillator, insulin pumps or metallic splinters, (vi) claustrophobia. MRI-compatible lenses are inserted on the

head coil for participants requiring visual correction.

6.1.2 Task. The virtual environment is developed with Unity® game engine

(Unity® Technologies, version: 2019.3.13f1, fig. 1 a-c). The environment is a grass-covered

circular arena (radius: 300 virtual units [vu]). The arena is surrounded by water forming

a natural, wall-free boundary. In the background, a mountain range with identifiable land-

marks (eg. castle, lighthouse, church, windmill, trees, houses, rocks) is visible. The intra-

maze object, a column (dimension: 6.5*6.65*23.22vu) is located 28.3 vu North-East off the

arena center. The participant experiences a first-person view (camera height: 13.4vu), with

a 60-degree field of view.

The task consists of ten blocks of nine trials, alternating between egocentric and allo-

centric conditions, for a total of 90 trials (fig. 1 e-h). A single trial is composed of a self-paced

free *navigation phase* to a starting location represented by a 4vu-wide red circle on the arena

ground, followed by the *orientation phase*, where participants get unlimited time to rotate in

place to orient themselves around the starting location. After pressing the response button,

the *trajectory phase* starts, where the participant is passively moved along a predefined path.

Trajectories lie at 3 possible distances ("close": 80vu, "medium": 115vu and "far": 160vu)

from the object and 3 possible directions to the object ("towards": 60°, "perpendicular": 90°

and "away": 120° away from straight ahead direction. The order of the trajectories across

different distances and directions are counterbalanced between blocks but not between par-

ticipants. Each trajectory is experienced twice, once in the egocentric condition and once in

the allocentric condition, to ensure a strictly similar visual experience between the two con-

ditions. At the end of the trajectory and after a 2-second black screen (*black screen phase*),

the participant has to point in the direction of the object, from an egocentric or allocentric

perspective (*response phase*). In the egocentric condition, participants are asked to indicate where the object is relative to her/his own perspective after they had been moved along the trajectory (i.e., ahead, left, right or behind them), while in the allocentric condition, participants must indicate where they are relative to the object at the end of the trajectory (i.e.,North, East, West, or South of the object). During the response phase, two response panels can be displayed: an egocentric response panel, where the circle-like coordinate system is centered on the person, and an allocentric response panel centered on the column. Participants use the response buttons to rotate an arrow to indicate their response. The *feedback phase* follows where 5 different smiley faces are displayed according to pointing error (from happy to sad faces in the degree range: [0-15], [15-35], [35-65], [65-110] and [100-180]). The next trial starts immediately after. At the beginning of a new block, a panel indicated whether an allocentric or egocentric trial is to be performed. Participants are instructed during the out-of-scanner training that the main distal landmark (the castle) corresponds to the arbitrary North of the island. During the training, participants are shown a top-down view of the arena and its distal landmarks.

In the control experiment, the column height is reduced to 1.82 vu (its length and width did not change). Besides the column height, the environment and task used in the normal and control experiments are strictly identical.

6.1.3 Human protocol. The whole experiment lasts 2.5 hours on average. After consenting, participants perform a training task for up to 30 minutes outside of the scanner. After going through the 7T-MRI safety checklist with the on-site radiographer, the participant is set in the Siemens 7.0 T MAGNETOM Terra scanner (NTNU Norwegian 7T MR Center, PTX head coil). Participants are equipped with earplugs and foam pads for ear pro-

tection and minimizing motion. Throughout the whole session, participants are instructed to maintain complete stillness. Structural scans are acquired before functional ones. Functional scans are divided into 10-minute runs, with in-between breaks. Since the task is self-paced and in-scanner time is no longer than 1.5 hours, some participants perform fewer than the 90 predefined trials. An MR-compatible eye-tracker (SR Research EyeLink 1000) records eye movements when participants perform the task. A 5-point calibration procedure is performed after structural scans and prior to beginning the task. During the task, gaze position are queried at 60 Hz and integrated into the Unity environment using the EyeLink Wrapper 2.0 plugin package[31] when saccades are detected. Eye movements could not be recorded when participants wear corrective lenses, leading to a valid subset of n=37/47 participants with valid eye-tracking data. The virtual environment was projected on a 32 inches diagonal LCD screen sitting at the back on the bore (Nordic Neurolab InRoom device), seen through a mirror spanning approximately 30° of visual angle. The participants used four-button response grip controller (Nordic Neurolab ResponseGrips) to move in the virtual environment. Three buttons are used for movement: forward movement, left rotation, and right rotation, and one button to indicate their response. After a compulsory break, participants perform two cognitive tests before debriefing with the experimenters: a computerized version of the Perspective Taking test[27] and the 4 Mountains test[38] (4MT).

For participants invited twice, the order of the normal and control experiments is counterbalanced. Data from this second session is not presented here.

6.1.4   fMRI acquisition parameters.   High-resolution T1-weighted images are acquired with an MP2RAGE sequence (Magnetization Prepared with 2 Rapid Gradient-Echoes), with following parameters: echo time=1.99ms, repetition time=4.3s, inversion time

1=840 ms, inversion time 2=2370 ms, voxel size=0.75mm^3, flip angle=5/6°, slice thickness=0.75mm, and a total of 224 sagittal slices.

BOLD T2*-weighted functional images are acquired with multi-band accelerated echo-planar sequence[30] and following parameters: TR=2s, TE=19 ms, flip angle=80°, voxel size=1.25mm isotropic, field of view (FoV)=200mm, 74 slices, GRAPPA multi-band acceleration factor=2, resulting in 288 volumes. Four volumes are acquired subsequently with reversed phase encoding direction for distortion correction.

6.1.5 Data preprocessing.

6.1.5.1 Behavioural data. Trial outliers were identified and removed from the behavioural data. Outliers corresponded here to any pointing error value that is more than three scaled median absolute deviations from the median, subject-wise.

6.1.5.2 Gaze data. Participant's 3D gaze data is smoothed using a 5ms moving window. The intersection points between the participant's gaze in Unity coordinates and the object, background, and ground are calculated using the MatGeom library. The colliders was a rectangular parallelepiped for the column (31*31*34.5 vu), a sphere for the background (radius: 300vu), and a circular surface the ground (radius: 300vu), centered on the arena terrain. Gaze positions from the orientation phase of the experiment only are used for calculating heatmaps. Heatmaps show intersections with the ground and the background only and are normalized across participants separately for the egocentric and allocentric conditions. Additionally, gaze time proportion is calculated as the number of gaze intersections falling in each category (column, background, or ground) divided by the total number of recorded gaze intersections, separately for the egocentric and allocentric conditions.

6.1.5.3   Neuroimaging data.   The T1-weighted background noise, typical of the

MP2RAGE sequence, is removed by multiplying the uni and inv2 images[20].   Subse-

quently, dcm2niix-converted[36] (version 2-November-2020), BIDS-organized data were pre-

processed with fmriprep[17] (version 23.0.2, RRID:SCR_016216), which is based on Nipype

1.8.6 (RRID:SCR_002502[22,23]).

B0 inhomogeneity mappings.   The B0-nonuniformity map (or fieldmap) is estimated

based on two (or more) echo-planar imaging (EPI) references with topup[3].

Anatomical data.   The T1-weighted (T1w) image is corrected for intensity non-

uniformity (INU) with N4BiasFieldCorrection[57], distributed with ANTs 2.3.3 (RRID:SCR_-

004757[4]), and used as T1w-reference throughout the workflow.   The T1w-reference is then

skull-stripped with a Nipype implementation of the antsBrainExtraction.sh workflow (from

ANTs), using OASIS30ANTs as target template. Brain tissue segmentation of cerebrospinal

fluid (CSF), white-matter (WM) and gray-matter (GM) is performed on the brain-extracted

T1w using fast (RRID:SCR_002823[61]).   Volume-based spatial normalization to one stan-

dard space (MNI152NLin2009cAsym) is performed through nonlinear registration with

antsRegistration (ANTs 2.3.3), using brain-extracted versions of both T1w reference and the

T1w template.   The following template is selected for spatial normalization and accessed

with TemplateFlow[11] (23.0.0): ICBM 152 Nonlinear Asymmetrical template version 2009c

(RRID:SCR_008796; TemplateFlow ID: MNI152NLin2009cAsym[18]).

Functional data.   For each BOLD runs, the following preprocessing is performed.

First, a reference volume and its skull-stripped version were generated by aligning and

averaging 1 single-band references (SBRefs).   Head-motion parameters with respect to the

BOLD reference (transformation matrices, and six corresponding rotation and translation

parameters) are estimated before any spatiotemporal filtering using mcflirt[32]. The estimated

fieldmap is then aligned with rigid-registration to the target EPI (echo-planar imaging) ref-

erence run. The field coefficients are mapped on to the reference EPI using the transform.

BOLD runs are slice-time corrected to 0.972s (0.5 of slice acquisition range 0s-1.95s) using

3dTshift from AFNI (RRID:SCR_005927[12]). The BOLD reference is then co-registered to the

T1w reference using mri_coreg (FreeSurfer) followed by flirt[32] with the boundary-based reg-

istration[24] cost-function. Co-registration is configured with six degrees of freedom. First, a

reference volume and its skull-stripped version are generated using a custom methodology of

fMRIPrep. Several confounding time-series are calculated based on the preprocessed BOLD:

framewise displacement (FD), DVARS and three region-wise global signals. FD was com-

puted using two formulations following Power et al. (absolute sum of relative motions[47]) and

Jenkinson et al. (relative root mean square displacement between affines,[32]). FD and DVARS

are calculated for each functional run, both using their implementations in Nipype (follow-

ing the definitions by[47]). The three global signals are extracted within the CSF, the WM,

and the whole-brain masks. Additionally, a set of physiological regressors were extracted

to allow for component-based noise correction (CompCor[6]). Principal components are esti-

mated after high-pass filtering the preprocessed BOLD time-series (using a discrete cosine

filter with 128s cut-off) for the two CompCor variants: temporal (tCompCor) and anatomi-

cal (aCompCor). tCompCor components are then calculated from the top 2% variable voxels

within the brain mask. For aCompCor, three probabilistic masks (CSF, WM and combined

CSF+WM) are generated in anatomical space. The implementation differs from that of Be-

hzadi et al. in that instead of eroding the masks by 2 pixels on BOLD space, a mask of

pixels that likely contain a volume fraction of GM is subtracted from the aCompCor masks.

This mask is obtained by thresholding the corresponding partial volume map at 0.05, and it ensures components are not extracted from voxels containing a minimal fraction of GM. Finally, these masks are resampled into BOLD space and binarized by thresholding at 0.99 (as in the original implementation). Components are also calculated separately within the WM and CSF masks. For each CompCor decomposition, the k components with the largest singular values are retained, such that the retained components' time series are sufficient to explain 50 percent of variance across the nuisance mask (CSF, WM, combined, or temporal). The remaining components are dropped from consideration. The head-motion estimates calculated in the correction step were also placed within the corresponding confounds file. The confound time series derived from head motion estimates and global signals were expanded with the inclusion of temporal derivatives and quadratic terms for each[49]. Frames that exceeded a threshold of 0.5 mm FD or 1.5 standardized DVARS were annotated as motion outliers. Additional nuisance timeseries are calculated by means of principal components analysis of the signal found within a thin band (crown) of voxels around the edge of the brain, as proposed by[45]. The BOLD time-series are resampled into standard space, generating a preprocessed BOLD run in MNI space. First, a reference volume and its skull-stripped version are generated using a custom methodology of fMRIPrep. All resamplings can be performed with a single interpolation step by composing all the pertinent transformations (i.e. head-motion transform matrices, susceptibility distortion correction when available, and co-registrations to anatomical and output spaces). Gridded (volumetric) resamplings are performed using antsApplyTransforms (ANTs), configured with Lanczos interpolation to minimize the smoothing effects of other kernels[34]. Non-gridded (surface) resamplings are performed using mri_vol2surf (FreeSurfer). Many internal operations of fMRIPrep use

Nilearn 0.9.1 (RRID:SCR_001362[1]), mostly within the functional processing workflow. For more details of the pipeline, see the section corresponding to workflows in fMRIPrep's documentation.

6.1.6 Regions of interest definition. Four regions of interest (ROIs) are chosen *a priori* for analysis: i) the entorhinal cortex, including both posterior-medial (pmEC) and anterior-lateral (alEC) subregions, as defined in Syversen et al.[53], ii) the hippocampus, including both posterior and anterior subregions and iii) parahippocampal cortex. Both the hippocampus and parahippocampal cortex ROIS are generated from individual participants' ASHS segmentation of the medial temporal lobe structures[59]. Each mask is transformed from native space into MNI space and resampled to EPI resolution using FSL FLIRT. To create group masks, participant-specific masks in MNI space are averaged, thresholded at 50%, and binarized using fslmaths. Finally, iv) the retrosplenial complex, we used a mask from Ramanoel et al.[48], comprising both RSC proper (Brodmann areas 29/30) and functional RSC (Brodmann areas 23/31).

6.1.7 fMRI analyses.

6.1.7.1 Overview. All analyses are performed in SPM12. Images are high-pass filtered with a 180-s cutoff. Nuisance regressors for the first-level models include six realignment parameters (x,y,z, pitch, roll, yaw) and their derivatives and quadratic terms, in-scanner motion spikes (defined as any data point over a framewise displacement of 0.9), and the average signal within individual brain mask or anatomically-derived eroded CSF and WM masks. Data are spatially smoothed with a Gaussian full-width-at-half-maximum kernel of 8mm. Out-of-brain voxels are excluded from the analyses.

6.1.7.2 Localization models. Stick functions sampled each second of the naviga-

tion phase similar to Spiers et al.[52], while parametric modulators for these regressors con-

tained either *i)* the egocentric direction to the object in the range [0,180] degrees, *ii)* the

allocentric direction to the object, with values in the range [0,360] degrees, and iii) distance-

to-goal values, in the range [0,220] vu. Each direction/distance values were rescaled onto

[1,-1] range, with 1 representing straight-ahead direction in the egocentric model, North di-

rection in the allocentric model and closest distance to the object in the distance model.

6.1.7.3 Tuning models. Egocentric, allocentric and distance values during the nav-

igation phase were discretized into 8 regressors, as shown in figures 3b-c, 4c-d and 6b-c. A

fine-grained allocentric tuning model (figure 4g) was evaluated with allocentric directions be-

ing discretized into 16 regressors representing 16 allocentric direction bins. Note that outlier

data points were removed before calculating group median in this fine-grained, thus more

noisy, model.

6.1.7.4 Additional models. The hemispheric lateralization model (figure 3i) was

estimated with egocentric direction remapped onto [1,-1] range, representing right and left

directions, respectively. The pure clover model (figures 4b and 7g) was estimated based on 2

regressors representing moments in time where the participant location coincides with on-

clover directions (bins 2, 4 ,6 and 8) or off-clover directions (bins 1, 3, 5 and 7 on figure 4c).

The visibility models (presented in figure 6e,g) were estimated separately for moments in

time where the object was visible to the subject, or not in sight. To account for the fact that

these models are estimated on half as much data points compared to the original model, we

choose to decrease the number of distance bins to 4.

6.1.8 Statistics for human data. Raw data were transformed with a Box–Cox

transformation to achieve normality[42] and outlier data points (defined as lower/higher than

1.5 inter-quartile range of the 25th or 75th distribution percentile) were removed. Nor-

mality of the data is verified by visual inspection of Q–Q plots. For repeated measure

ANOVAs, degrees of freedom of the factor ($df_{(factor)}$ = k-1) and the error ($df_{(error)}$ = $df_{(factor)}$

x $df_{(subject)}$) are presented, with ($df_{(subject)}$ = N-1). Greenhouse-Geisser correction is applied

when Mauchly's Test for sphericity is significant, hence affecting the degrees of freedom of

the omnibus tests reported in the text. The generalized eta-squared ($ges\eta_g^2$) is used as as

effect size. When appropriate, the four first polynomial contrasts were estimated, evaluating

linear, quadratic, cubic and quartic tendencies in the data. When normality and homoscedas-

ticity were dubious, Wilcoxon signed rank test was used to compare paired data. Effect size

for non-parametric tests were calculated as a correlation coefficient r, as $r = zscore/\sqrt{n}$. Al-

pha level for statistical significance was set at P < 0.05. Posthoc tests were evaluated with

a Bonferroni correction. Exact p-values are reported, until p<0.0001. Statistical tests were

one-sided.

6.2   Rodent experiments

6.2.1   Animals and surgery. An adult female Long Evans rat, 3 months old, was

used for single unit recordings. The animal was housed in an enriched cage with 3 other

female litter mates. One week prior to surgery, the rat was moved to an individual cage (45

x 44 x 30 cm) to allow for acclimation and, following surgery, to prevent potential damage

to the probe implant. The animal was housed in a temperature- and humidity-controlled

facility and kept on a reversed 12-hour light–dark cycle. All experiments were conducted

during the dark phase. The animal either maintained its baseline weight or experienced weight gain during the experiments and had ad libitum access to food and water, both before and during behavioral experiments. All experimental and surgical procedures were carried out in compliance with the Norwegian Welfare Act and the European Convention for the Protection of Vertebrate Animals used for Experimental and other Scientific Purposes.

During the surgical procedure, the animal was initially anesthetized in a ventilated Plexiglas chamber using 5% isoflurane vapor. Anesthesia levels were then adjusted to 1.0–2.5% isoflurane throughout the surgery to maintain an appropriate depth of anesthesia. Body temperature was kept at 37°C with a heating pad. After the animal was fully anesthetized, subcutaneous injections of analgesics were administered: Metacam (meloxicam; 2.5 mg/kg) and Temgesic (buprenorphine; 0.05 mg/kg). Additionally, local anesthesia with 0.5% Marcain was applied under the scalp before making the surgical incision. The surgical site on the skull was prepared by exposing the area and sterilizing it with 0.9% saline and 3% hydrogen peroxide. Using a high-speed dental drill with an 0.8 mm burr, openings were made in the skull for the placement of skull screws and craniotomies above retrosplenial cortex based on predetermined coordinates. To provide a stable electrical reference, a stainless steel bone-tapping screw was securely inserted into the skull, serving as the ground and electrical reference for subsequent recordings. A Neuropixels 1.0 probe (IMEC) was stereotactically inserted into the right hemisphere of the rat, with electrical contacts oriented toward lambda. The insertion targeted the tissue spanning from the retrosplenial cortex to the superior colliculus, based on coordinates relative to bregma: AP -5.6 mm and ML 0.5 mm. External reference and ground wires were attached to a skull screw positioned in the left hemisphere at AP -1 mm and ML +2 mm, and sealed with SCP03B Silver Conduc-

tive Paint Bottle from Elfa. The probe outside the brain was air-sealed using bead-sterilized

Vaseline and enclosed within a custom-designed, 3D-printed black plastic housing. The im-

plant was secured with Venusflow (Unident AS) cured under UV light and black-dyed dental

cement to minimize light-induced electrical interference.

Postoperative care included administering subcutaneous fluids, analgesics, and allow-

ing the animal to recover in a heated 37 ° C chamber for 1 to 2 hours prior to recording.

6.2.2   Recording and behavioural training.   The animal was handled extensively

for 3-5 weeks prior to the experiment to ensure acclimation to the experimenter. Following

the handling period, the rat was habituated to a black 150*150*50 cm recording arena over

several days before undergoing surgery and recording sessions. The recording environment

included the arena itself, a white cue card positioned on the north wall (fig. 5b), and a

hardware setup located on the south wall. The recording environment was kept at consistent

as possible throughout the experimental period.

The animal was introduced to the object and habituated previously so that it was fa-

miliar during the recording sessions. Neural data were collected during open-field foraging

sessions (2 x 20 minutes each) in which the rat freely foraged for corn puff crumbs scattered

on the arena floor by the experimenter. For the object session, the object was placed in the

northeast quadrant of the box, and a similar protocol as the open field session was used (2 x

20 minute sessions). Each block of the task consisted of an open field session followed by the

object session to ensure complete coverage of the arena in each condition.

6.2.3   Data analysis.   In vivo electrophysiological hardware included Neuropixels

1.0 Probes (IMEC), a National Instruments PXIe-1071 chassis and a PXI-6133 I/O module for

recording analog and digital input[33]. The implanted probes were connected via a headstage

circuit board and an interface cable positioned above the head of the animal. Excess cable was counterbalanced using elastic string to ensure that the animal could move freely throughout the experimental arena.

Neural data were recorded with SpikeGLX acquisition software (Janelia Research Campus). Amplifier gain settings were configured at 500× for recording spikes and 250× for local field potential (LFP). An external reference and an AP filter were set with a cutoff frequency of 300 Hz. Culster cutting and spike sorting was performed using Kilosort4[44]. During each recording session, signals were collected from Bank 1, mapping 385 channels.

6.2.3.1 GLM-based cell classification. To identify neurons with allocentric vectorial tuning to objects, we employed a Generalized Linear Model (GLM)-based statistical framework as described in detail in Mimica et al.[37]. This framework was used to evaluate the neural responses of recorded cells to specific behavioral and spatial features. Neural spike data were modeled as a function of the position of the animal, allocentric object distance and angle to the animal (and their derivatives), egocentric distance and angle to the object from the animal (and their derivatives), and other kinematic features such as turning and running speed.

The model selection process involved three steps: *i) Feature selection:* features related to animal-object vector relationships were extracted from behavioral data using a combination of 3D motion capture analysis, as outlined in Mimica et al.[37]. These features included allocentric position of the animal relative to the object (allocentric head angle, distance to the object and their 1st derivatives) and egocentric object-animal proximity (egocentric head angle and distance to the object calculated from the nose of the animal and their 1st derivatives) and angular speed. *ii) GLM fitting:* neural spike trains were modeled using a Bernoulli

family GLM, where the probability of spiking was predicted based on the selected behavioral features. 10 fold cross-validation was applied to ensure robust model fitting and avoid over-fitting; *iii) Model evaluation:* the goodness-of-fit for each GLM was assessed using metrics including deviance, pseudo-R2, and log-likelihood ratios. Neurons were classified as exhibiting allocentric vectorial tuning to the object if their firing rates showed significant modulation by allocentric object proximity features, as determined by the likelihood ratio test ($p < 0.05$).

6.2.3.2 Data processing. The set of neurons identified by the GLM as having allocentric vectorial tuning to the object had to meet 3 further criteria, such that cells with potentially spurious or non-specific responses were removed where possible. These criteria included: *i)* Goodness-of-Fit threshold: only neurons with a pseudo-R2 above a predefined threshold (0.1) were retained. *ii)* significant tuning: neurons had to exhibit statistically significant tuning curves for allocentric features to the object. *iii)* firing rates: to reduce the occurrence of spurious or nonspecific responses, neurons with mean firing rates below 2Hz were excluded, as were neurons with mean rates above 20Hz. Neurons with mean firing rates below 2 Hz often fire too sparsely for reliable tuning estimates, and those above 20 Hz can reflect overly high, potentially nonspecific activity. Restricting to 2–20 Hz helps reduce spurious tuning and ensures a more consistent physiological range.

6.2.3.3 Single neuron firing rate. Spiking rates were normalized by occupancy time in each spatial bin, with spatial and temporal binning of spiking activity as follows:

$$r(x,y) = \frac{n_{\text{spikes}}(x,y)}{t_{\text{occupancy}}(x,y)} \tag{1}$$

where $r(x,y)$ is the firing rate in a specific bin defined by spatial coordinates (x,y), $n_{\text{spikes}}(x,y)$ is the number of spikes recorded in that bin, and $t_{\text{occupancy}}(x,y)$ is the total time spent in that

694   bin.

695   **6.2.3.4   Population median firing rate across neurons.**   After calculating firing

696   rate maps for individual neurons, we computed the median firing rate across all neurons at

697   each bin location to summarize population activity:

$$\text{median\_firing\_rate}(x, y) = \text{median}(r_1(x, y), r_2(x, y), ..., r_N(x, y)) \tag{2}$$

698   where $r_i(x, y)$ represents the firing rate of neuron i in bin (x, y), and N is the total number of

699   neurons. This approach allows for a robust estimation of the central tendency of firing rates

700   across the population and is less sensitive to outliers compared to the population mean. The

701   standard error of the mean (SEM) was calculated to quantify variability in firing rates as

702   follows:

$$\text{SEM} = \frac{\sigma}{\sqrt{N}} \tag{3}$$

703   where σ is the standard deviation of the firing rates across cells, and N is the total number

704   of cells. For time points with missing data, the standard deviation was calculated excluding

705   NaN values. Both the median firing rates and SEM were then smoothed with a Gaussian

706   kernel:

$$\text{smoothed\_data} = \text{gaussian\_filter1d}(\text{data}, \sigma) \tag{4}$$

707   where $\sigma = 0.75$ for firing rates and $\sigma = 0.1$ for SEM.

708   **6.2.3.5   Peak detection algorithm.**   The peak detection process involved the fol-

709   lowing steps: First, each neuron's 2D firing rate matrix was normalized to ensure consistent

710   detection across cells with varying firing rate ranges:

$$\text{normalized\_matrix} = \frac{\text{matrix} - \text{min}(\text{matrix})}{\text{max}(\text{matrix}) - \text{min}(\text{matrix})} \tag{5}$$

Second, a dynamic threshold was calculated for each neuron based on its maximum normalized firing rate:

$$\text{dynamic\_threshold} = 0.8 \times \max(\text{normalized\_matrix}) \qquad (6)$$

Third, the `peak_local_max` function from the `skimage.feature` module was used to detect local maxima in the normalized matrix. Parameters included the `min_distance`, set to 5 (in matrix indices) to ensure spatial separation between peaks, `threshold_abs`, set to the calculated dynamic threshold and the `exclude_border`, set to False to allow detection of peaks near matrix edges. Fourth, detected peaks were sorted by intensity in descending order, and the top 4 peaks were selected as significant. Finally, peak coordinates were converted from matrix indices to actual angle and distance values using predefined bin centers. This allowed for systematic identification of preferred firing directions and distances for each neuron, features relevant to their allocentric vectorial properties.

6.2.4   Statistics for rodent data.   The Kolmogorov-Smirnov (K-S) test was used to compare the similarity between one distribution and a shuffled version of itself. We report the KS statistic, or D statistic, which is the maximum absolute difference between the cumulative distribution functions. The D value is a measure of the test effect size, as it represents how far apart the two distributions are (range from 0 to 1).

6.2.5   Histology.   After the recordings were completed, the rat was euthanized with an overdose of isoflurane, followed by intracardial perfusion with saline and 4% paraformaldehyde. The probe shank was left in the brain and the entire skull was immersed in 4% paraformaldehyde for 24 hours. The next day, the brain was carefully extracted from the skull and placed in a 2% dimethyl sulfoxide (DMSO, VWR, USA) solution for cryoprotection, lasting one to two days before cryosectioning.

Following cryoprotection, the brain was frozen and sectioned coronally in three se-
ries of 40 μm slices using a freezing sliding microtome (Microm HM-430, Thermo Scien-
tific, Waltham, MA). The first series of sections was mounted directly onto Superfrost slides
(Fisher Scientific, Goteborg, Sweden). Hoechst staining was performed to confirm anatomical
probe placement (Fig. supp. S3).

All brain sections were digitized using a digital scanner equipped with appropriate
illumination wavelengths and scanning software provided by Carl Zeiss AS (Oslo, Norway).
The resulting images were analyzed and visualized using ZEN (Blue Edition) software.

Probe placement and channel counts in cortical sub-regions were estimated using the
HERBS (Histological E-data Registration in rodent Brain Spaces) software toolbox[19], which
allowed for precise alignment of electrode tracks in histological sections and subsequent map-
ping of recording sites in each region.

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8   Author contributions

M.B., I.M.K. and C.F.D. designed the human experiments. M.B., P.S. and J.R.W. designed the rodent experiments. M.B., I.M.K. and P.S. collected and analyzed the data. M.B., I.M.K., P.S., J.R.W., C.F.D. wrote the article.

9   Conflict of interest

The authors declare no competing interest.

10   Data availability statement

The fMRI data supporting the findings of this study were collected in accordance with Norwegian data protection and privacy regulations. Due to legal and ethical restrictions imposed by the Norwegian Data Protection Authority (Datatilsynet) and the Regional Committees for Medical and Health Research Ethics (REK), the raw imaging data cannot be shared publicly. Data access is therefore limited to approved research collaborators who have obtained the necessary ethical approvals and data handling agreements in Norway. Interested researchers may contact the corresponding author to discuss potential collaborations under these constraints. Additionally, group-level brain maps and individual tuning curves supporting figs. 3,4,6,7, as well as behavioural data supporting fig. 2 (position and eye movement time series, task performance) and the raw rodent data supporting fig. 5 will be made available on the following repository (https://osf.io/5t49x/) at the time of publication.

11   Code availability statement

The Matlab code used to model and analysis the fMRI data, as well as behavioural analyses scripts will be made available on the following repository (https://osf.io/5t49x/) at the time of publication.

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