Ligand-dependent G protein dynamics underlying opioid signaling efficacy

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Abstract

Activation of heterotrimeric G proteins by G protein-coupled receptors (GPCRs) requires large-scale opening of the Gα α-helical domain (AHD) to expose the nucleotide-binding site and facilitate GDP–GTP exchange. While orthosteric ligands are known to modulate GPCR conformation and signaling efficacy, how these effects propagate to the G protein itself remains unclear. Using single-molecule fluorescence resonance energy transfer (smFRET) imaging, we monitored AHD motions in G_i proteins coupled to the µ-opioid receptor (µOR) across a spectrum of ligand- and nucleotide-bound states. We find that receptor ligands differentially modulate these dynamics from over 70 Å away, with higher-efficacy agonists more effectively promoting transitions to an open, low-nucleotide-affinity conformation. These data also capture transient µOR-G_i intermediates during nucleotide binding and suggest that µ-opioid ligand efficacy arises in part from allosteric control over G protein conformational equilibria that kinetically gate activation.

Main

Full and partial agonists have distinct therapeutic applications for targeting opioid receptors, with full agonists used in pain management and partial agonists in treatment of opioid use disorder. µ-opioid receptors (µORs) are GPCRs that mediate analgesia and reward responses to common opioid drugs by catalyzing guanine nucleotide exchange in heterotrimeric G_i proteins, composed of Gα, Gβ, and Gγ subunits[1]. When activated by ligands, µOR and other class A GPCRs couple to inactive, GDP-bound G proteins at their intracellular surface (Fig. 1a). This interaction induces conformational changes in the G protein that promote GDP release and GTP binding, activating the G protein and triggering downstream signaling cascades which effectuate the physiological response[2]. Recent biophysical evidence indicates that ligands modulate GPCR signaling by stabilizing distinct receptor conformational states that vary in their G protein coupling efficiency[3–9]. However, the extent to which these ligand-dependent states propagate to the coupled G protein remains unclear, and if they do, whether these altered G protein conformational states also affect signaling outcomes in the cell.

The most significant conformational change observed for G protein activation by a GPCR is the separation of its Ras-like and α-helical domains (RLD and AHD) in the Gα subunit (Fig. 1a,b), as revealed by early double electron-electron resonance (DEER) spectroscopy[10] and X-ray crystallography[11] studies. In all inactive-state crystal structures, the AHD – a six α-helical bundle (αA-αF) – packs against the RLD, burying the bound GDP in the interface between the domains[12]. Following receptor coupling and GDP release, this interface opens by tens of angstroms[10,11,13–15], resulting in an intrinsically dynamic AHD that has largely eluded high-resolution structural characterization[16].

Fig. 1 | Intrinsic G protein conformational dynamics facilitate μOR-G$_i$ activation. a, Agonist binding to a class A GPCR promotes G protein coupling and activation via GDP-GTP exchange. The activation rate can be influenced by the rate of initial receptor-G protein coupling (i) or through modulating the G protein conformational changes that facilitate nucleotide exchange (ii). **b**, Labeling sites R90C (green) and E238C (magenta) shown on superimposed Gα$_i$ structures in the inactive (GDP-bound) state (PDB: 1GP2) and in the receptor-coupled (nucleotide-free) state with an open AHD (PDB: 7L0Q). **c**, Ligand efficacy profiles determined from Gα$_i$Δ6-90C/238C GTP turnover assay (Methods). Error bars denote 95% c.i., three technical replicates; *p < 0.023, **p < 0.004 and p > 0.058 (ns), two-sided, unpaired t-test with Bonferroni correction. BUP, buprenorphine; MOP, morphine; LFT, lofentanil. **d**, Schematic of smFRET experiments. **e**, Example single-molecule fluorescence (top) and FRET (bottom) time traces of surface-tethered μOR-G$_i$ bound to full agonist lofentanil, displaying transitions between a low-FRET, open state and a high-FRET, closed state. **f**, Transition density plot displaying the mean FRET values before (x-axis) and after (y-axis) each transition for lofentanil-μOR-G$_i$ (scale bar, 10^{-3} transitions per bin per second; n_t total transitions).

Multiple lines of evidence suggest that AHD movements are critical for facilitating GDP-GTP exchange
across all G protein isoforms, yet their role in signaling efficacy remains poorly understood[17]. While
molecular dynamics (MD) simulations indicate that domain separation alone may not be sufficient for
nucleotide exchange, a variety of functional[18–20], spectroscopic[13,21,22], and computational[23,24] studies
demonstrate that AHD movements are tightly linked to both GDP release and the subsequent binding of
GTP[16,25,26]. Here, we use total internal reflection fluorescence (TIRF) smFRET imaging to directly monitor
AHD motions in G$_{i1}$ proteins bound to μ-opioid receptor (μOR) activated by diverse orthosteric ligands,
both in the absence and presence of nucleotide. Our results reveal how ligand-specific signals are
allosterically encoded in the G protein conformational ensemble; a pattern that generalized to G$_i$ bound to
neurotensin type 1 receptor (NTSR1). These data suggest a mechanistic basis for opioid signaling
efficacy that extends beyond simple receptor-G protein coupling efficiency.

Results

Donor and acceptor fluorophores (LD555[27] and JFX673[28], respectively) were stochastically labeled on the
AHD (R90C) and RLD (E238C) of a previously reported minimal cysteine Gα$_{i1}$ mutant[10,29] (Fig. 1b and
Extended Data Fig. 1a; Methods). This construct, Gα$_i$Δ6-90C/238C, exhibited a WT-like pattern of ligand
efficacy-dependent GTP turnover with μOR in vitro (Fig. 1c), and LD555/JFX673-labeled Gα$_i$Δ6-90C/238C
heterotrimers efficiently coupled to agonist-bound μOR, forming stable, nucleotide-depleted ternary
complexes (Extended Data Fig. 1b). For TIRF imaging (Methods), these μOR-G$_i$ ternary complexes were

specifically immobilized on quartz slides with an M1 fab fragment (Fig. 1d and Extended Data Fig. 1c),
remaining functional on the surface as tested by the ability for GTPγS-induced G protein dissociation
(Extended Data Fig. 1d). Time-dependent changes in AHD position were captured from smFRET
trajectories of individual, immobilized µOR-G_i complexes, which displayed reversible transitions (on the
order of 1 s^{-1}) between low- and high-FRET states (Fig. 1e,f). These dynamics reflect spontaneous
domain separation and re-engagement consistent with the various poses observed in previous negative
stain and cryo-electron microscopy (cryo-EM) studies of a receptor-G protein complex[16,26].

Ligand-induced AHD opening

We examined the impacts of µOR bound to ligands with varying signaling efficacies (Fig. 1c), as well as
the unliganded (apo) receptor, on AHD dynamics in coupled G_i heterotrimers (Fig. 2a and Extended Data
Fig. 2a). These ligands included strong full agonists lofentanil and BU72[30], the endogenous enkephalin-
like full agonist DAMGO, the partial agonist morphine, and weaker partial agonists buprenorphine and
mitragynine pseudoindoxyl (MP). Population FRET efficiencies for all ligands showed two predominant
states, centered at ~0.27 and ~0.62, along with a minor ~0.47 FRET population that remained constant
across all samples. At µOR bound to full agonists, occupancy of the low-FRET (0.27) state increased
relative to partial agonists, whereas that of the high-FRET (0.62) state decreased (Fig. 2a). This ligand-
induced low-FRET occupancy was strongly correlated with in vitro GTP turnover activity (a direct measure
of efficacy) (R^2 = 0.97; Fig. 2b), indicative of an open Gα conformation like that seen in active-state
complex structures[11,14] (see Fig. 1b). Likewise, unliganded (apo) µOR was the least efficient at stabilizing
this low-FRET, open conformation, in line with its slow GTP turnover under basal conditions (Fig. 2a,b). In
addition, the apo complex exhibited a small population (~10%) from excursions to >0.7 FRET, a state
which the AHD rarely sampled under liganded conditions (Fig. 2a and Extended Data Fig. 2a).

To investigate the kinetics of AHD motions within µOR-G_i, we used hidden Markov modeling (HHM) to
idealize the traces and quantify transitions between high- and low-FRET states (Figs. 1e and 2c;
Methods). The occupancy of the mid-FRET (~0.47) state was not ligand-dependent (Fig. 2a) and was
sampled transiently, with nearly half of its occurrences lasting two frames or less (≤100 ms). Hence, the
mid-FRET state may reflect an unstable conformational intermediate and/or result from time-averaging of
rapid (>10 s^{-1}) low-to-high FRET excursions at the current imaging speed. Because neither mid-FRET
transitions nor distributions could be clearly distinguished from the high-FRET state at the ensemble level
(Extended Data Fig. 2b and Fig. 2a), we analyzed the kinetics as a two-state system, where the mid- and
the high-FRET states are collapsed into a single, broadly distributed (~0.4-0.6) closed conformation.

This analysis revealed that increasing ligand efficacy at µOR enhances the overall level of dynamics
within coupled G_i heterotrimers (Fig. 2c and Extended Data Fig. 2b,c), primarily by reducing the duration
that the AHD dwelled in the closed, high-FRET state (Extended Data Fig. 2c). Mean dwell times in this
high-FRET state (τ_{high}) depended strongly on ligand efficacy (R^2 = 0.96; Fig. 2d), with the apparent rate of
AHD opening being approximately 2.5-fold faster for lofentanil- compared to apo-occupied complexes (ca.
0.9 s^{-1} and 0.36 s^{-1}, respectively). Conversely, dwell times in the low-FRET state were similar (ca. 1.4 s on
average) across all ligands tested (R^2 = 0.17; Fig. 2d and Extended Data Fig. 2c). Thus, ligand-dependent
shifts in the AHD's conformational equilibrium (Fig. 2a) stem from the destabilization of its closed state,
rather than stabilization of the open, domain-separated conformation. This indicates that efficacy is, at
least in part, dependent on the ability of the ligand to allosterically initiate domain separation rather than
merely to promote receptor conformations that affect initial G protein coupling.

While domain separation is key for receptor-catalyzed GDP release, the observed high-to-low FRET
transition rates are slower (approximately 10-fold) than expected from G protein activation measurements
in living cells (<100-300 ms)[31,32]. However, the absolute values of these rates may be influenced by
experimental conditions, such as the detergent micelle, cysteine mutations, temperature, and/or
limitations in imaging speed and fluorescent probes. Parallel smFRET imaging of NTSR1-G_i ternary

Fig. 2 | AHD opening is ligand efficacy-dependent. a, Population FRET efficiency histograms for surface-tethered μOR-G_i ternary complexes with three-state gaussian mixture model (GMM) fits showing the open (red) and closed (cyan) states (n, number of traces). Error bands, s.d. of GMM fits from 100 bootstrap samples of the FRET traces. **b**, Scatter plot of ensemble average low-FRET, open-state occupancies and mean GTP turnover activities observed for each ligand with log-linear fit (dashed line; R^2 = 0.97). Errors represent 95% c.i. **c**, Example FRET (blue) and predicted state (red) traces for partial (top; buprenorphine) and full (bottom; lofentanil) agonists. **d**, Mean dwell times in the low-FRET, open and high-FRET, closed states; data is mean ± s.d., 100 bootstrap samples of the idealized traces.

complexes (Methods), which couple promiscuously in vitro, yielded a similar correlation between agonist-induced low-FRET occupancy and GTP turnover (R^2 = 0.89; Extended Data Figs. 3 and 4; cf. Fig. 2b). The addition of SBI-553, an allosteric modulator shown to elicit an effector-dependent response[33], shifted the AHD toward the open state proportionally to its positive modulation of GTP turnover in vitro (Extended Data Fig. 3b). These findings suggest that AHD displacement may be a general determinant of ligand efficacy across G protein-receptor pairs, consistent with previous bioluminescence resonance energy transfer (BRET) studies showing distinct G protein conformational signatures for different calcitonin and α2-adrenergic receptor ligands[22,34].

G protein dynamics in the basal state

In basal (inactive)-state structures of heterotrimeric G proteins, the Gα AHD tightly encloses the bound GDP[35,36]. Yet spontaneous domain separation must occur to permit GDP release, as G proteins still slowly exchange nucleotide even without GPCR catalysis[37]. To investigate these basal dynamics, we

immobilized labeled G_i heterotrimers via an N-terminal histidine-tag and imaged their AHD motions in a
physiological concentration of GDP (30 µM[38]) (Extended Data Fig. 5a; Methods). Compared to receptor-
bound G protein, we observed more conformational heterogeneity (≥3-4 distinct states) and reduced
average interdomain separation, primarily due to the AHD sampling an additional (inactive, high-FRET)
state centered at ~0.77 (Extended Data Fig. 5b-d). This inactive state corresponds to an interdye distance
consistent with full domain closure (Δopen-closed ≈ 28 Å; Methods) and likely resembles the GDP-bound
conformation seen in the inactive-state G_i crystal structure[35] (see Fig. 1b). These data predict that even in
its "closed," 0.62 high-FRET state, the receptor coupled G_i AHD remains partially displaced (ca. 5-8 Å).
Elimination of the fully-closed (0.77 FRET) conformation upon agonist-stimulated receptor-G protein
complex assembly (Fig. 2a and Extended Data Fig. 3a) is likely related to the mechanism of GDP release
(or simply the absence of bound GDP).

Under basal conditions, individual G_i AHD exhibited reduced dynamics but still transitioned to the open
state (ca. 0.15 s^{-1}; Extended Data Fig. 5c,d), consistent with prior MD simulations[23]. These transitions
predominantly traveled through a mid-FRET (~0.5) intermediate state (Extended Data Fig. 5d),
suggesting that a partially open AHD may mediate transitions between GDP-bound and GDP-unbound
conformations. Introducing an alanine substitution at residue R144 in the α subunit (Extended Data Fig.
5e), previously shown to destabilize the RLD-AHD interaction and enhanced basal nucleotide
exchange[37,39], shifted the AHD from the fully closed to open states, resulting in dynamics similar to,
though still slower than, the receptor-bound G protein (Extended Data Fig. 5f-h).

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Nucleotide effects on intact µOR-G_i complexes
As described above, the AHD can adopt at least four distinct FRET states: (i) a low-FRET, open state
(~0.27) that correlates with ligand efficacy; (ii) a short-lived, intermediate state (~0.47); (iii) a high-FRET,
closed state (~0.62) while the G protein is receptor-bound; and (iv) an inactive, GDP-bound closed state
(~0.77) seen basally in uncoupled G_i. The FRET states observed in receptor-coupled G proteins (0.27,
0.47, and 0.62) could not be directly linked to stable nucleotide binding, as GTP or GDP delivery caused
rapid dissociation from the receptor, precluding equilibrium observation of bound states (Fig. 3a).
However, GMP and pyrophosphate (PPi) (Extended Data Fig. 6a), which together mimic GTP binding in
the nucleotide pocket of small G proteins[40], did not significantly dissociate the complex (Fig. 3a,b).

Using this approach with surface-tethered µOR-Gi complexes activated by DAMGO (Fig. 3c-f and
Extended Data Fig. 6b-e), we observed a concentration-dependent shift from open to closed states
induced by 0.1-100 µM GMP·PPi (Fig. 3c and Extended Data Fig. 6b). This is consistent with previous
reports that domain closure is required for triphosphate nucleotide binding[25,41] and reflects GMP·PPi
binding through stabilization of the high-FRET closed conformation rather than an acceleration of domain
closure (Extended Data Fig. 6c). The GMP·PPi-induced transitions also exhibited ligand-specific
differences: complexes with the lower-efficacy ligand morphine (Fig. 3d and Extended Data Fig. 6f-h)
showed heightened sensitivity to GMP·PPi (EC$_{50}$ = 0.28 µM) compared to those with DAMGO (EC$_{50}$ =
1.45 µM) (Fig. 3d). This difference aligns with the ligand-dependent energetic biases for AHD closure, as
evident from their conformational equilibriums before nucleotide binding (Fig. 2a). Importantly, even at the
highest GMP·PPi concentrations tested (≥10 µM), transitions to the basal (~0.77 FRET) state remained
rare (Extended Data Figs. 6b,f and 7a,b), suggesting receptor coupling restricts access to the fully closed
conformation of the AHD regardless of nucleotide.

Further analysis of individual smFRET traces (Extended Data Figs. 6d,g and 7a,b) revealed stepwise
transitions through a partially open, mid-FRET state (~0.4–0.5) within both DAMGO- and morphine-bound
complexes (Fig. 3e and Extended Data Fig. 6h). GMP·PPi-induced stabilization of this intermediate was
weaker in DAMGO-bound complexes, which unlike morphine, maintained some apparent direct
transitions between low- and high-FRET states even at saturating nucleotide concentrations (Fig. 3e).
However, synchronization analysis revealed a brief (1-2 frame) mid-FRET dwell during many of these
domain separation events (Fig. 3f, cf. Extended Data Fig. 6e). We had also observed stepwise transitions
in heterotrimeric G_i with GDP present (Fig. 5d), consistent with a prior smFRET study linking the partial
domain separation in the mid-FRET state to an intermediate level of nucleotide affinity[21].

Fig. 3 | Nucleotide binding promotes AHD closure through an intermediate. a, GTPγS, but GMP with PPi, dissociates G protein from surface-tethered μOR. Error bars, mean ± 95% c.i. (n = 3-6 movies of the same sample) of FRET particles remaining after delivery of 10 μM nucleotide or buffer (vehicle); p = 0.23 (ns), two-sided, unpaired t-test. **b**, Schematic of single-molecule GMP·PPi titration experiments. **c**, Population FRET efficiency histograms (symbols) with b-spline fits (lines) for DAMGO-bound μOR-G_i in the presence of increasing concentrations of GMP·PPi. **d**, Apparent EC_{50} values measured from GMP·PPi-induced ensemble average low-FRET occupancy for DAMGO (blue) and morphine (gray); error bars, s.d. of 100 bootstrap samples of the FRET traces (3,341 molecules total across all conditions). Lines are fits to dose response functions (Hill slope = 1.0). **e,f**, Transition density plot (**e**) for DAMGO with 10 μM GMP·PPi (scale bar, 10^{-3} transitions per bin per second; n_t total transitions) and contour plot of synchronized high-to-low transitions (**f**) showing a short-lived dwell in a mid-FRET state (yellow box, width ≈ one frame) (cf. Extended Data Fig. 6e).

Together, these findings suggest a mechanism where nucleotide contacts are broken or formed progressively rather than all at once, providing a free-energy-efficient pathway for nucleotide exchange via a transient intermediate step[42,43]. Similar accessibility of this binding-competent intermediate in the nucleotide-free state seen across ligands (Fig. 2a) may allow for selective modulation of GDP release (i.e., by tuning high-FRET state stability) without as drastically affecting GTP binding between ligands.

Discussion

We have shown that opioid ligand efficacy extends beyond initial receptor-G protein coupling to include the modulation of G protein conformational equilibria within the fully formed signaling complex. These results demonstrate that the G protein conformation can be dynamically tuned by the GPCR, sampling a continuum of distinct states rather than merely discrete 'off' or 'on' conformations (Fig. 2b). While these insights advance our understanding of opioid drug action – informing efforts to develop safer analgesics[44–47] – they also suggest a broader framework for how interplay between receptor and effector conformational states can influence the signaling response amplitude, which has clinical implications across GPCR targets[48,49].

Our findings reveal that ligand-dependent conformational changes propagate from the receptor to the
engaged G protein, modulating its AHD between open, closed, and transient intermediate states.
Consistent with the loss of contacts upon separation of the Gα domains, measurements showed that the
high-FRET (closed) state corresponds to higher nucleotide affinity, while the low-FRET (open) state
possess reduced affinity (Fig. 3c,d). This aligns with prior findings that mutations to the interdomain
interface or hinge regions accelerate basal nucleotide exchange[37,50–52], and that increased interdomain
motion correlates with G protein activation[53–55]. Thus, the energetic bias towards AHD opening observed
in full agonist-bound complexes (Fig. 2a and Extended Data Fig. 3a) suggests a reduction in nucleotide
affinity, driven by the shift in the G protein conformational equilibria.

To test this, we measured GTPγS binding to nucleotide-free µOR-G$_i$ complexes by fluorescence
dequenching (Methods). Buprenorphine-occupied complexes exhibited 1.5-fold faster GTPγS binding
than those bound to the full agonist lofentanil (Fig. 5a), consistent with extensive earlier evidence that
higher-efficacy ligands reduce the nucleotide affinity of coupled G proteins[5,56–61]. Although this initially
appears to contradict in vivo signaling patterns, measurements under more physiological conditions –
where both GDP and GTP are present – showed a reversal in binding kinetics (Fig. 5a), with GDP
competition dramatically slowing GTPγS binding to buprenorphine-bound complexes[62].

In the cytoplasm, where GTP is ~10-fold more abundant than GDP, G protein activation is primarily limited
by GDP release, as GTP loading occurs rapidly afterward. Full agonists promote AHD opening, facilitating
GDP release and efficient GTP binding. In contrast, partial agonists restrict open-state occupancy,
favoring GDP retention or rebinding, which prolongs its residence time in the interdomain pocket. This
competitively inhibits GTP binding and thereby delays G protein activation, ultimately explaining why
partial agonists exhibit lower signaling efficacy despite faster intrinsic GTPγS binding rates (Fig. 5a). The
relative difference between ligands is also greater for GDP than for GTP binding, further suggesting that
G protein dynamics are primarily selected to regulate the GDP release step.

Fig. 4 | Model for the role of G protein dynamics in ligand-dependent signaling. a, Binding of BODIPY-conjugated GTPγS (GTPγS-BDP-FL) to nucleotide-free µOR-G$_i$ containing unlabeled Gα$_i$Δ6-90/238C subunit was monitored via fluorescence dequenching for lofentanil (top) and buprenorphine (bottom). Normalized kinetic spectra in the absence (gray) or presence (red) of GDP were fit using exponential association to obtain the mean association time (*t*; dashed lines). **b**, Engagement of µOR intracellular surface by the Gα$_i$ α5 helix destabilizes the α1 helix and disrupts the interdomain interface (dashed outline) composed of αF, α1, L1, and the n-terminal segment of αA. Structures shown: 1GP2 (blue) and 7T2H (orange). **c**, Schematic of main FRET states and their proposed relation to α5 insertion efficiency and nucleotide (NT) binding. Full agonists favor a more open G protein complex (left), lowering nucleotide affinity. Partial agonists promote greater domain closure (right), increasing the energetic barrier for nucleotide release and reducing the likelihood of progressing to the nucleotide-free complex required for activation.

At a structural level, these ligand-induced G protein conformational changes require allosteric
communication spanning over 70 Å from the receptor's orthosteric site to the G protein AHD. Differences
in G protein dynamics observed with different orthosteric ligands can be understood as alterations in the

complementarity between the binding surfaces where the RLD and AHD meet. While GPCR-mediated G
protein activation is known to involve remodeling of the α5 helix in the Gα subunit[63–66], studies also link
this helix to AHD opening[10,23,67] – minimally through the α1 helix in the RLD[68,69] (Fig. 5b). The α1 helix
directly connects to the AHD via the αA helix and helps stabilizes the inactive G protein conformation
through conserved interdomain contacts with αF and the hinge region[70]. During GPCR engagement, α5
moves away from the nucleotide-binding pocket toward the intracellular vestibule of the receptor, causing
rotation and partial disorder of α1. These rearrangements sterically disrupt the interdomain interface,
opening the AHD and priming the ternary complex for GDP release[13,15,66] (Fig. 5b).

Recent smFRET and DEER studies of β2 adrenergic and μOR receptors showed that full agonists
promote greater outward movement of transmembrane helix 6 (TM6)[5,6], expanding the intracellular
vestibule where α5 binds. This TM6 displacement, along with other ligand-dependent changes to the
receptor's cytosolic surface, may facilitate AHD opening by making it more energetically favorable for G
protein to bind[15,71–73]. In contrast, partial agonists have been shown to induce less efficient α5 insertion[74],
which could weaken α1-mediated disruption of the Gα interdomain interface and prolong the dwell time in
the high-FRET, high-nucleotide-affinity state preceding GDP release (Fig. 5c). This mechanism helps
explain an earlier observation that partial agonists at β2-G$_s$ act to stabilize transient, GDP-bound GPCR-
G protein intermediates[5], which could function as kinetic traps retarding productive complex assembly
and activation. As for the low-affinity open state, the similar low-FRET dwell times observed across opioid
agonists (Fig. 2d) suggest that once the AHD is fully open, ligand identity has minimal influence on its
dynamics – possibly because the AHD is affixed against Gβ, as seen in a recent cryo-EM structure[14].

Unlike real-time insights from smFRET, resolution of the AHD in cryo-EM studies of GPCR-G protein
complexes is limited by the conformational heterogeneity imaged upon freezing[16,55]. As such, it may be
unsurprising that structures with ligands of varying efficacies tend to show minimal differences in
Gα[57,75,76], capturing only lowest-energy conformations while even subtle changes at the interdomain
interface can significantly alter domain separation dynamics[70]. By revealing that GPCRs allosterically
control nucleotide exchange through biasing the conformational equilibria of the AHD, our work provides
mechanistic evidence for how opioid and other GPCRs function as guanine nucleotide exchange
factors[17]. This dynamic framework provides a more complete picture of GPCR signal transduction and
suggests new strategies for developing opioid therapeutics with optimized efficacy profiles and potentially
fewer adverse side effects.

Methods

Minimal cysteine Gα$_i$ expression, purification, and labeling
Mutations R90C and E238C were introduced into a previously published[29] minimal cysteine background
(C3S, C66A, C214S, C350S, C325A, C351I) of human Gα$_{i1}$ containing an N-terminal 6x histidine-tag prior
to a rhinovirus 3C protease site. This construct (Gα$_{i1}$Δ6-90C/238C) was expressed in BL21 cells using
pET21a and purified as previously described[77]. Briefly, cells grown in Terrific Broth were induced with 0.5
mM IPTG at an OD$_{600}$ of 0.6 and harvested after 15-20 hours at room temperature. The harvested cells
were resuspended in lysis buffer (50 mM HEPES pH 7.4, 100 mM sodium chloride, 1 mM magnesium
chloride, 50 μM GDP, 5 mM beta-mercaptoethanol, 5 mM imidazole, lysozyme, and PIs) and disrupted via
sonication. Intact cells and cell debris were removed by centrifugation and Gα$_i$ was purified from the
supernatant using Ni-NTA resin. The protein was eluted using 200 mM imidazole in lysis buffer and
dialyzed with 1:1000 w/w 3C protease at 4 °C overnight to cleave the histidine tag. 3C protease, cleaved
histidine tag and unreacted protein was removed using fresh Ni-NTA and the flow-through containing
purified Gα was concentrated and polished using size exclusion chromatography (SEC) on a Superdex
200 10/300 GL column (Cytiva) in G protein buffer (20 mM HEPES pH 7.4, 100 mM sodium chloride
(NaCl), 1 mM magnesium chloride, 20 μM GDP, and 100 uM TCEP). For preparation of His-tagged Gα$_i$,
the Ni-NTA elute was concentrated and further purified using SEC without the intervening 3C cleavage
step. The R144A mutant of Gα$_{i1}$Δ6-90C/238C was purified with an intact His-tag in the same manner.

Aliquots of Gα$_i$ were flash frozen in liquid nitrogen at a concentration of approximately 200 μM in 20 %
glycerol as a cryoprotectant.

For site-specific labeling, fluorophores were attached stochastically to C90 and C238 in Gα$_i$Δ6-90C/238C
under conditions designed to minimize off-site labeling (Extended Data Fig. 1a). Aliquots of frozen,
purified Gα were brought to room temperature and diluted to a concentration of 30 μM in G protein buffer
containing 50 μM GDP. Maleimide-conjugated LD555 (Lumidyne Technologies) and JFX673peg$_4$ (Janelia
Fluor) were added simultaneously, at a 2- and 1.7-fold molar excess, and incubated in the dark at room
temperature for 30 minutes. The reaction was quenched by 5 mM L-Cysteine (Sigma) before labeled
protein was purified from the unreacted dyes using a Superdex 200 column in buffer containing 20 mM
HEPES pH 7.4, 100 mM NaCl, 1 mM MgCl$_2$, 20 μM GDP, and 100 uM TCEP. On average, labeling
efficiency was >80%, with an LD555:JFX673 ratio of <1. SEC-pure, dye-labeled Gα$_i$ was concentrated,
and flash frozen at approximately 60 μM for future use.

Purification of Gβγ
Gβγ heterodimer was expressed in *Tni* cells using a baculovirus generated by the BestBac (Expression
systems) method and purified as described previously[23]. Briefly, we used a single virus containing the
genes for both the Gβ$_1$ and Gγ$_2$ subunits. A N-terminal 6x histidine tag followed by a 3C protease site was
contained in the sequence of Gβ to be used for Ni affinity purification. Gβγ heterodimer was extracted
from the membrane using a dounce homogenizer in solubilization buffer containing 20 mM HEPES pH
7.4, 100 mM NaCl, 1.0% sodium cholate, 0.05% dodecylmaltoside (DDM, Anatrace), 5 mM beta-
mercaptoethanol, and PIs. After removing insoluble debris, the protein was washed with a solubilization
buffer in batch and gradually exchanged from sodium cholate to 0.1% DDM on Ni-NTA resin. The elute
was dialyzed with 3C protease to cleave the histidine tag as we described for Gα$_i$. Cleaved Gβγ was
dephosphorylated and further purified on a MonoQ 10/100 GL column (GE Healthcare) using a linear
gradient of NaCl (50-250 mM). The main peak containing prenylated Gβγ was dialyzed into 20 mM
HEPES pH 7.4, 100 mM NaCl, and 0.02% DDM and flash frozen in liquid nitrogen at a concentration of
150 μM with 20% glycerol as a cryoprotectant.

Formation dye-labeled G$_i$ heterotrimer
Purified Gβγ heterodimer was exchanged into buffer containing 20 mM HEPES pH 7.4, 100 mM NaCl, 1
mM magnesium chloride, 50 μM GDP, and 100 uM TCEP using a 30k MWCO centrifugal protein
concentrator (Thermo Scientific) and mixed with approximately 0.25 molar equivalents of dye-labeled
Gα$_i$Δ6-90C/238C-6x histidine (2.5 μM Gαi final concentration). Buffer exchange was performed until the
final concentration of DDM during heterotrimer formation was << the sub critical micellar concentration
(CMC). After incubation at room temperature for 0.5 hours, unbound Gβγ heterodimers were removed
coincident with surface immobilization for smFRET imaging by pulling down the heterotrimer on
microscope slides coated in anti-His epitope tag antibodies. Unlabeled, wild-type human G$_i$ heterotrimer
(Gα$_{i1}$β$_1$γ$_2$) was co-expressed and purified from *Hi5* insect cells as previously described[23].

Purification of μOR
Mouse μOR was expressed in *sf9* insect cells using the baculovirus method (Expression systems) in the
presence of the opioid antagonist naloxone (Sigma Aldrich). We used a modified *Mus musculus* sequence
containing an N-terminal Flag tag and an 8x histidine tag in front of a rhinovirus 3C protease site on the
C-terminus. μOR was expressed and purified in the presence of 10 μM naloxone as has been previously
described[78]. Briefly, *sf9* cells were infected at a density of 4 x 10^6 ml^{-1} and incubated for 48 hours at 27
°C. Cell membrane was solubilized in DMM and 3-[(3-cholamidopropyl)-dimethylammonio]-1-propane
sulfonate] (CHAPS, Anatrace) and purified by immobilized metal affinity chromatography using Ni-NTA
resin. The elute was loaded onto M1 anti-Flag immunoaffinity resin and gradually exchanged into a buffer
containing naloxone, 0.01% lauryl maltose neopentyl glycol (L-MNG, Anatrace) and 0.001% cholesterol
hemisuccinate (CHS, Steraloids). The receptor was further purified on SEC in a buffer containing no
ligand, 25 mM HEPES pH 7.4, 100 mM NaCl, 0.02% L-MNG and 0.002% CHS. The peak containing the
now unliganded μOR (Extended Data Fig. 1b, dashed line) was concentrated to ~100 μM, supplemented

with 20% glycerol, and flash frozen for later use.

Assembly of µOR-G$_i$

To prepare µOR-G$_i$ ternary complexes for smFRET, µOR was equilibrated in a 5-10 molar excess of
opioid agonist for 10 minutes at room temperature. After pre-incubation of untagged Gα$_i$ and Gβγ on ice
for 30 minutes, they were mixed with liganded receptor at a 1:1.2:1 (Gα$_i$:Gβγ:µOR) molar ratio. The final
concentration of receptor during complexing was ~2.5 µM and the buffer adjusted to contain 20 mM
HEPES pH 7.4, 100 mM NaCl, 0.01% L-MNG, 0.001% CHS, 100 µM TCEP, 50 µM GDP and 1 mM
MgCl$_2$. Complex assembly progressed for one hour at room temperature to reach steady state, after
which 25 mU ml^{-1} Apyrase (New England Biolabs) was added and incubated overnight at 4 °C. The
apyrase-stabilized complex was supplemented with 2 mM CaCl$_2$ and loaded onto a M1 anti-Flag
immunoaffinity column at room temperature. The column was washed with 20 column volumes (CV) of
complex buffer (20 mM HEPES pH 7.4, 100 mM NaCl, 0.01% L-MNG, 0.001% CHS and 1-10 µM ligand)
containing 2 mM CaCl$_2$ before the protein was eluted using 200 µg ml^{-1} Flag peptide (DYKDDDDK) and 2
mM EDTA. The elute was further purified using a room temperature Superdex 200 10/300 SEC column in
complex buffer containing 0.1-1 µM ligand. Peak fractions corresponding to monodispersed µOR-G$_i$ were
concentrated to ~3 µM and supplemented with 20% glycerol before flash freezing in liquid nitrogen.
Single-use aliquots were stored at -80 °C until imaging. Nearly identical FRET efficiency distributions were
obtained using complexes that had not been frozen (data not shown). Given that the unliganded µOR-G$_i$
complex showed reduced stability at room temperature, all chromatography and sample preparation for
the apo was performed at 4 °C.

Purification and assembly of labeled NTSR1-G$_i$

Full-length human NTSR1 was expressed and purified as previously described[79]. In brief, an NTSR1
sequence modified with an N-terminal Flag tag followed by an octa-histidine tag was expressed in *sf9*
cells using a baculovirus. Solubilized cells were purified using sequential Ni-NTA, anti-Flag and SEC
columns into a final buffer containing 20 mM HEPES, pH 7.4, 100 mM NaCl, 0.0025% L-MNG, 0.00025%
CHS and 0.1 µM NTS$_{8–13}$ (acetate salt, Sigma). Peak fractions were concentrated to 200 µM and flash
frozen and stored at -80 °C.

Ternary complexes of NTSR1-G$_i$ were assembled and purified as described for µOR with a few
modifications. Purified NTSR1 in 0.1 µM NTS$_{8–13}$ was loaded onto an anti-Flag column and exchanged
into different orthosteric ligands (NTR1-17 or CGX-1160) by washing for 0.5 hours (~15 CV) at room
temperature with buffer containing 1 µM of the new ligand and 20 mM HEPES, pH 7.4, 100 mM NaCl,
0.0025% L-MNG, and 0.00025% CHS. Flag peptide and EDTA were removed from the elute using a 7k
MWCO desalting spin column (Thermo Scientific) before the NTSR1 was concentrated and used for
complexing. To couple to the receptor, labeled Gα$_i$Δ6-90/238C and Gβγ were first assembled into
heterotrimer as described above and were mixed with NTSR1 in an ~1:1 ratio following incubation.
Complexing then progressed as for liganded µOR-G$_i$ using buffers containing NTSR1 ligands.

GTP turnover assays

Analysis of GTP turnover was performed using a modified GTPase-Glo™ assay (Promega) as described
previously[5]. We started the reaction by mixing purified, unliganded or ligand-bound µOR or NTSR1 and G$_i$
protein in an assay buffer containing 20 mM HEPES, pH 7.5, 100 mM NaCl, 0.01% L-MNG, 0.001% CHS,
100 µM TCEP, 10 mM MgCl2, 10 µM GDP, 5 µM GTP and saturating concentrations of receptor ligands.
After incubation for 90 minutes, reconstituted GTPase-Glo™ reagent was added to the sample and
incubated for 30 minutes at room temperature. Luminescence was measured after the addition of
detection reagent and incubation for 10 minutes at room temperature using a SpectraMax Paradigm plate
reader. Measurements were performed in triplicate on the same plate and reported as the mean relative
light units (RLU) normalized to DAMGO or NTS$_{8-13}$. Ligand efficacy profiles were determined from the
GTP turnover activity stimulated by µOR or NTSR1, using Δ6-90C/238C and WT Gα$_i$ constructs,
respectively. Basal G$_i$-dependent GTP turnover was measured using buffer without any receptor and a

120-minute incubation period.

smFRET measurements

Data was acquired using a lab-built prism-based TIRF microscope. LD555 (donor) and JFX673-peg$_4$
(acceptor) labeled Gα$_i$-Δ6-90/238C was excited using a 532 nm solid-state laser (Coherent OBIS™ LS
Laser) set to 40 mW at the laser. Photons emitted from LD555 and JFX673 were collected through a 1.27
NA 60x water-immersion objective (Nikon) and split onto two cooled EMCCD cameras (Andor iXon Ultra
888) connected by a 640 nm dichroic mirror (ZT640rdc, Chroma) housed in a TwinCam™ (Cairn). All
imaging was performed at 19 °C and movies were recorded with Andor Solis (i) software (Andor) at a 50
ms time resolution (20 frames s^{-1} (fps)). Microfluidic chambers for smFRET imaging were constructed
from passivated quartz slides and coverslips using a modified protocol from Ha et. al[80]. Briefly, aminated
glass surfaces passivated with mPEG-SVA (MW 5000; Laysan Bio Inc.) doped with 0.6% w/w biotin-PEG-
SVA (MW 5000; Laysan Bio Inc.) were exposed to two additional rounds of passivation reactions using
only mPEG-SVA.

For experiments with receptor-G$_i$ ternary complexes, passivated imaging chambers were incubated for 5
minutes with 0.2 mg ml^{-1} NeutrAvidin (Thermo Scientific), followed by 5 minutes with 25 nM biotinylated
anti-Flag M1 Fab fragment. Unbound M1 Fab and NeutrAvidin were washed out using imaging buffer (20
mM HEPES, pH 7.5, 100 mM NaCl, 0.01% L-MNG, 0.001% CHS, 2 mM CaCl$_2$). Fluorophore-labeled
µOR-G$_i$ and NTSR1-G$_i$ complexes were filtered using a 0.22 µm PVDF membrane (Millipore Sigma) and
loaded onto the microscope slide at 200 pM by pulling down the N-terminal Flag tag on the receptor.
Unbound complexes were washed out at an immobilization density of ~0.1 molecules µm^2. All
experiments were performed in imaging buffer containing a saturating concentration of the orthosteric
and/or allosteric ligand. For smFRET of basal G$_i$ heterotrimer, NeutrAvidin-coated chambers were
incubated for 5 minutes with 0.02 mg ml^{-1} biotinylated anti-mouse IgG1 antibody (Abcam) followed by 5
minutes with 0.02 mg ml^{-1} mouse anti-hexa-histidine epitope tag antibody (Abcam). Purified,
LD555/JFX673peg$_4$-labeled G$_i$ with an uncleaved N-terminal hexa-histidine tag on the α subunit was
loaded onto the microscope slide at ~200 pM and measured in imaging buffer containing 30 µM GDP, 1
mM MgCl$_2$ and 100 µM TCEP. Anti-his tag immobilization has been reported previously[81,82] and was
specific (data not shown).

smFRET data analysis

Fluorescence time trajectories of single molecules were extracted from the movies and processed using a
custom software suite implemented in MATLAB which is available on GitHub. Donor traces were scaled
by a constant factor (γ) to account for the apparent unequal fluorophore brightnesses, calculated as γ =
ΔI_A/ΔI_D, where ΔI_A and ΔI_D are the changes in donor and acceptor intensity after acceptor photobleaching,
respectively[83]. FRET trajectories were calculated as $(1 + (γI_D/I_A))^{-1}$, where I_D and I_A are the background-
corrected donor and acceptor fluorescence intensities at each frame. FRET traces lasting at least 0.5 s
were selected for analysis that exhibited: (i) single-step photobleaching, (ii) overall anti-correlated donor
and acceptor intensities, (iii) a signal-to-noise ratio (SNR) (mean/s.d. of the total fluorescence intensity
before photobleaching) greater than 2, and (iv) acceptor photobleaching and/or low-FRET states with an
average FRET of at least ~0.2 (i.e., 1-2 s.d. from the center of the crosstalk distribution created by donor
leakage into the acceptor channel). All traces were manually inspected for the final datasets, which had a
geometric average SNR of ~11 across all samples. Population histograms summed over the first 3 s of
the selected FRET traces were fit to a mixture of 3-4 gaussian functions to derive the mean FRET values
and occupancies of each state. Initial guesses for the states were obtained from fitting the full agonists.
Errors for the gaussian mixture and state occupancies were calculated as the s.d. of 100 bootstrap
samples of the FRET traces (95% c.i. were obtained from 1.96 multiplied by s.d.).

FRET traces were idealized using a two- or three-state hidden Markov model (HMM) as implemented in
the vbFRET software[84]. The idealized FRET traces (viterbi) were clustered using a gaussian mixture to
remove overfitting of fluctuations within the same FRET state, and the resulting state sequences were
used to calculate transition density plots (TDPs) from transitions corresponding to ΔFRET$_{ideal}$ > 0.1. The
number of states k for each condition was determined based on the lowest value for which a $k + 1$ state

HMM fit did not change the clusters in a TDP of the uncorrected traces. To explore the exchange kinetics
between the fully open and closed FRET states within µOR-G$_i$, the state sequences resulting from a two-
state HMM and gaussian mixture fit were concatenated ("stitched") and the dwell times in each state were
extracted from the change points. Population dwell time distributions were calculated using a kernel
density estimate (smoothing bandwidth = 2x Scott's rule[85]) which was normalized to reflect the frequency
of dwells in time bins along the x-axis[86]. The mean lifetime in each state was estimated as the integral of
the normalized dwell-time survival curves restricted to < 30 seconds. Dwell times and their distributions
are reported as the mean ± s.d. from 100 bootstrap samples of the FRET traces, where the resampling
probability of each trace is weighted by its relative duration, as described previously[87]. As each
bootstrapped sample has a different randomly selected order of traces, this source of variability is
averaged over and reflected in the reported errors.

Synchronization plots of the high-to-low transitions in DAMGO-µOR-G$_i$ were calculated from clustering the
viterbi to two-states and selecting transitions from above to below the intermediate state center (~0.45).
While kinetics were analyzed with only γ correction, conversions of FRET efficiency to relative inter-dye
distances utilized additional corrections for channel crosstalk and direct acceptor excitation, as outlined
by Hellenkamp et al[88]. Figure preparation and downstream analysis of the selected FRET and idealized
trajectories were performed using custom scripts in python.

Bodipy-GTPγS binding assay
Binding of Bodipy conjugated GTPγS (GTPγS-BDP-FL, Jena Bioscience) to nucleotide-free µOR-G$_i$
complexes was measured as previously described (*91*). Briefly, complexes of ligand-bound µOR,
unlabeled Gα$_i$-Δ6-90/238C and Gβγ were purified by anti-Flag and added at a final concentration of
500nM to a 500 µL quartz cuvette containing 1 µM GTPγS-BDP-FL. Fluorescence was recorded at 512
nm (495 nm excitation) for 500 s at room temperature using a Fluorolog spectrophotometer (HORIBA)
with magnetic stirring. All experiments were performed in a buffer containing saturating ligands and 20
mM HEPES pH 7.4, 100 mM NaCl, 0.01% L-MNG, 0.001% CHS, 2mM MgCl$_2$ and 100 µM TCEP. Mean
association times for GTPγS-BDP-FL binding were calculated from resulting kinetic spectra by fitting a
pseudo first-order association function using non-linear regression in Python. We note that the C325A
mutation contained in the Δ6 cysteine construct affects the rate of spontaneous GDP release but
reportedly not GTP binding[89].

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Author contributions

470 JD, DH, JJ, RVS, CS, SC and BKK designed the single molecule experiments. JD, JJ and DH purified
471 proteins, while JD labeled the proteins and prepared complexes for imaging. JD performed nucleotide
472 turnover and binding assays. JD and RVS collected single-molecule data and analyzed it. RVS, JD and
473 SC developed the imaging platform and code. JD, RVS and BKK wrote the manuscript and interpreted
474 the results with input from all authors. RVS and BKK supervised the project.

Competing interests
476 BKK is a co-founder and consultant for ConfometRx, Inc. RVS is the director of drug discovery at
477 Greenstone Biosciences.

479   **Correspondence and requests for materials** should be addressed to Brian Kobilka.

Data availability statement
482   The data supporting the findings of this study are available from the corresponding authors after
483   publication. No unique materials or reagents were generated.

Code availability
486   Custom MATLAB code used for smFRET data processing is available at:
487   https://github.com/JonathanDeutsch/Freton.

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Extended Data Figures

Extended Data Fig. 1 | smFRET experimental controls. a, Site-specific labeling: SDS-PAGE analysis of purified Gα$_i$Δ6 'cys-less' background with and without engineered cysteines (R90C/E238C) labeled with either LD555 (left) or JFX673 (right) visualized using fluorescence imaging (top; 532 nm or 633 nm illumination), with Coomassie staining (bottom) as a gel-loading control. **b**, Representative room-temperature size exclusion chromatography (SEC) profiles of buprenorphine-bound µOR alone (dashed line) and as a ternary complex with dye-labeled G$_i$ heterotrimer (absorption in gray; LD555 fluorescence in green). **c**, Specificity of M1 fab-mediated immobilization: Uptake of 200 pM labeled µOR-G$_i$ onto passivated quartz slides coated with M1 fab fragment (blue; specific) and without M1 fab (gray; non-specific) recorded using 100 ms TIRF imaging at low laser power (1 mW at the source) to prevent photobleaching. **d**, Histogram of immobilized FRET particles (mean ± 95% c.i., n = 3 movies of the same sample) remaining after injection of buffer (vehicle) or 10 µM GTPγS into the imaging chamber shows GTPγS binding and functional dissociation of µOR-G$_i$ on the surface.

Extended Data Fig. 2 | **Analysis of AHD opening and closing in µOR-G$_i$. a**, Sample fluorescence
(LD555 in green and JFX673 in magenta; units, 10^4 counts) and FRET efficiency time traces for M1-Fab-
immobilized µOR-G$_i$ complexes in the indicated ligand and unliganded states. **b**, Transition density plots
displaying the mean FRET values before (x-axis) and after (y-axis) each transition (n_t total transitions per
condition) for a representative selection of the tested ligands. Scale bar, 10^{-3} transitions per bin per
second. **c**, Dwell time distributions of the µOR-G$_i$ AHD in the open, low-FRET state (top) and closed, high-
FRET state (bottom). Error bars, mean ± s.d. of 100 bootstrap samples of the FRET traces.

Extended Data Fig. 3 | Ligand-induced AHD separation in NTSR1-G$_i$. a, Population FRET efficiency histograms for surface-tethered NTSR1-G$_i$ ternary complexes bound to the indicated ligands, with three-state GMM fits showing the closed (green) and open (cyan and red) states (*n*, number of traces). Error bands, s.d. of the GMM fits from 100 bootstrap samples of the FRET traces. **b**, Correlation scatter plot of ensemble low-FRET, open-state occupancy versus log mean GTP turnover activity (three technical replicates) with $R^2 = 0.89$. Error bars, 95% c.i.; error band, bootstrapped 95% c.i. of the regression estimate. Ligands include the full agonist NTS$_{8-13}$, the active fragment of the neurotensin peptide; contulakin-G (CGX-1160), a glycopeptide derivative of NTS found in cone snail toxin; TC-NTR1-17 (NTR1-17), a synthetic partial agonist; SBI-553, an allosteric modulator.

Extended Data Fig. 4 | Example smFRET traces of the NTSR1-G$_i$ AHD. Example donor and acceptor fluorescence (LD555 in green; JFX673 in magenta) and FRET traces for surface-tethered NTSR1-G$_i$ bound to the indicated orthosteric and allosteric ligands.

Extended Data Fig. 5 | AHD dynamics in the basal state. a, Labeled Gα$_i$Δ6-90C/238C heterotrimers were tethered to quartz slides via an N-terminal His tag on the Gα subunit and a biotin-mouse antibody bridge. TIRF imaging of the surface-tethered G$_i$ AHD, without and with an alanine substitution at R144, was performed in physiologic 30 μM GDP. **b-d**, Population FRET efficiency histogram (squares; n, number of traces) with spline and four-state GMM fits (black and colored lines, respectively) (**b**), example FRET and predicted state traces (**c**), and transition density plot for the parent ('WT') construct (**d**). **e**, Structure of GDP-bound Gα$_{i1}$ (PDB: 1GP2) showing R144 contacts stabilizing the inactive, closed state at the distal interdomain interface. **f,** Population FRET efficiency histogram (circles) from imaging R144A shows a low-FRET shift relative to WT (red lines are high-FRET gaussians with percent occupancy from four-state fits). **g,h**, Example smFRET trace (**g**) and transition density plot (**h**) showing the effects of R144A on AHD dynamics. Pink lines are overlays of major transition density contours generated by a receptor-G protein ('R-G') complex (BU72-μOR-G$_i$). Scale bar, 10^{-3} transitions per bin per second (cf. Extended Data Fig. 2b).

Extended Data Fig. 6 | Additional data from imaging μOR-G$_i$ with GMP·PPi. Surface-tethered μOR-G$_i$ was imaged in a buffer containing various concentrations of equimolar GMP and PP$_i$ with either DAMGO- or morphine-occupied receptors. **a**, Structure of PPi and GMP. **b-d**, Population FRET histograms (**b**), dwell time distributions (two state model; see supplementary information) (**c**), and example fluorescence and smFRET traces (**d**; 10 μM GMP·PPi) from experiments imaging DAMGO-μOR-G$_i$. **e**, Synchronization plot of high-to-low transitions in the nucleotide-free state for DAMGO-occupied complex (cf. Fig. 3f). **f**, Population FRET histograms from titration experiments with morphine (MOP). **g,h**, smFRET trace (**g**) and transition density plot (**h**) in saturating (10 μM) GMP·PPi from experiments with morphine-bound μOR. Errors are mean ± s.d. of 100 bootstrap samples of the traces.

Extended Data Fig. 7 | Example smFRET traces with GMP·PPi. a,b, Sample trace recordings of the
fluorescence (LD555 in green and JFX673 in magenta; units, 10^4 counts) and FRET efficiency from
experiments imaging surface-tethered μOR-G_i bound DAMGO (**a**) and MOP (**b**) in buffer containing the
indicated concentrations of equimolar GMP and PPi.