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Cortical GABAergic inhibition dynamics around hippocampal sharp-wave ripples

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Abstract

Cortical inhibition, mediated by GABA, is essential in balancing excitation and modulating neural processing, but it is unclear to what extent inhibitory dynamics are responsive to internally generated hippocampal activity, such as sharp-wave ripples (SWRs). Employing widefield imaging of extracellular GABA with iGABASnFR2 and hippocampal recordings, we characterized cortical inhibition during sleep–awake states and in the neighborhood of SWRs. Sleep–awake transitions drastically reorganized cortical levels of GABA, with increased inhibition in wakefulness and decreased upon entering NREM sleep. In the neighborhood of SWRs, inhibition was state- and region-specific: during NREM, medial cortices (e.g., retrosplenial) increased GABA before SWRs, whereas sensory areas in the lateral cortices decreased it; during wake, GABA increased in lateral cortices after SWRs. These findings reveal that cortical inhibition is not static and ubiquitous but instead is dynamically characterized by brain state, orchestrating the flow of hippocampal outputs to the rest of the cortex. Inhibitory modulation, as our data reveal, forms a mechanism allowing selective gating of memory-related activity during wakefulness and sleep.

Keywords: Cortical inhibition, GABA dynamics, Sharp-wave ripples, Brain state transitions, Hippocampal–cortical communication

Introduction

Cortical function is revealed as a balance of excitation and inhibition that together determines the dynamics of neural circuits and behavior [1]. Excitatory neurons produce the majority of the cortical output and communicate long distance between brain regions [2]. Such excitatory flow must be modulated to ensure stable network, accurate construction of information, and adaptive behavioral output [3]. Inhibitory interneurons, about 20–30% of the cortical neurons, govern circuit excitability, neuron responsiveness, as well as rhythmic network activity during brain states [4-5]. Of the inhibitory interneurons, three subtypes of GABA-releasing interneurons have been distinguished: parvalbumin-expressing (PV+), somatostatin-expressing (SST+), as well as vasoactive intestinal peptide-expressing (VIP+) interneurons [5-7]. PV+ interneurons that target the perisomatic of the pyramids are the fast spikers that contribute to feedforward inhibition [8]. Acting rapidly to turn down pyramidal activity with millisecond fidelity, they enhance temporal fidelity to maintain

gamma oscillation [9-10]. SST+ interneurons, on the other hand, innervate distal dendrites, acting

feedback inhibition that reduces top-down as well as long-range integrative processing [11-13]. VIP+

interneurons, in turn, inhibit others of their kind, SST+ in particular, to recruit dis-inhibitory

circuits to maintain pyramidal neuron output during behavioral demands such as attention or level

of arousal change [14-16]. All in all, inhibition in no respect constitutes the easy opposite of excitation,

but rather an operating mechanism that constrains computation by spatially and temporally

distinctive control [1]. Inhibitory action chooses synaptic plasticity, tunes excitatory drive, and

synchronizes distributed communication of cortical areas [6]. E/I balance dynamically varies in

correspondence with sleep, wake, attention, and locomotion [17]. Inhibition disruption has been

implicated in a broad spectrum of neuropsychiatric illnesses like epilepsy, autism spectrum

disorder, and schizophrenia [18]. In this type of situation, it is preferable to have an idea of how

cortical GABAergic inhibition is regulated by internally self-generated hippocampal activity

patterns like sharp-wave ripples (SWRs), as they are indeed built to synchronize brain-wide

communication in sleep as well as quiet wakefulness.

Recent studies have started to answer this question by describing excitatory cortical activity in

response to hippocampal SWRs. A study using genetically encoded glutamate sensors indicated

that cortical excitatory activity was strongly modulated by SWRs in a state-dependent manner.

Karimi Abadchi et al. [19-20] demonstrated that, during NREM sleep, the SWRs precede a period of

suppression in the whole cortex that is followed by sequential activation originating in medial and

in visual cortices, areas involved in the default mode system. During quiet wakefulness, however,

SWRs are followed by robust suppression in agranular retrosplenial cortex, with late rebound in

cortical glutamatergic activity. These studies demonstrate that SWRs have organized and state-

specific excitatory patterns of excitation as their outcome. Cortical computation, however, is

almost never regulated by excitation in isolation. Since excitatory drive is generally followed or

accompanied by inhibition [1,6], the state-dependent patterns of excitation during SWRs thus

inevitably bring to the forefront the question of the corresponding inhibitory patterns. Thus, to this

point, whereas excitatory responses have been accurately described, the inhibitory aspect of the

cortical responses to SWRs has remained to a great extent uninvestigated. It is important to know

how it is that GABAergic inhibition plays its part in this process, since the generation of the timing,

spread, and functional significance of the cortical activation is controlled by the regulatory action

of the inhibition mechanisms.

Here, we attempt to fill this gap; in the process, we combine widefield imaging of the genetically
encoded GABA sensor iGABASnFR2 [21] with hippocampal electrophysiology to track GABAergic
dynamics in the dorsal cortex during different states of the brain such as NREM, REM, and wake.
We first establish the baseline by describing the spontaneous cortical GABA transients during
these states, against which to gauge state-dependent GABAergic inhibition. We then inquired
whether SWRs shape cortical GABAergic inhibition in time- as opposed to space-ordered patterns,
as one would expect should hippocampal memory-related activity be selectively modulated by
distributed inhibitory processes. Emphasizing the inhibitory aspect of the cortical response to
SWRs, our study attempts to reveal a level of cortico-hippocampal organization that exists but
moves beyond the level of the excitatory to the level of the inhibitory circuits that defines the flow
of information across the brain.

Materials and methods

Animals and experimental conditions

We employed eight adult (>2 months) EMX-Cre female and male mice of the C57BL/6J strain for
imaging studies. For studying natural sleep, EMX-Cre mice were injected intracranially with AAV
vectors in a Cre-dependent manner to drive the expression of the genetically encoded GABA
sensor iGABASnFR2 in neocortical and hippocampal excitatory neurons. This enabled optical
reporting of extracellular GABA in excitatory cortical circuits. Strong expression of
iGABASnFR2 in targeted brain areas was validated through brain sectioning analysis as outlined
in our previous publication [22]. Mice were group-housed (two to five mice) under a 12-hour light-
dark cycle and had ad libitum access to water and a standard laboratory mouse diet. For sleep
recording studies, mice were singly housed after head-plate and electrode implantation surgery.
All animal studies were approved by the University of Lethbridge Animal Care Committee and
adhered to the Canadian Council for Animal Care guidelines.

Viral constructs and retro-orbital injection procedure

To enable selective detection of extracellular GABA dynamics in excitatory cortical circuits, we
used EMX-Cre transgenic mice, in which Cre recombinase is primarily expressed in excitatory
pyramidal neurons of the neocortex and hippocampus. This allowed for Cre-dependent expression

of genetically encoded sensors specifically in those neurons. Two AAV vectors were used:
AAV2/PHP.N-Syn-flex-iGABASnFR2, encoding the Cre-dependent GABA sensor, and
AAV2/PHP.N-Syn-flex-cpSFGFP, a non-sensing cytosolic GFP control. Both constructs were
obtained from the Canadian Neurophotonics Platform Viral Vector Core (RRID: SCR_016477)
and purified to a final concentration of 1.5×10^{13} genome copies per milliliter (GC mL^{-1}). Retro-
orbital injections [23]which outlines systemic delivery using the PHP.N capsid [24]. The animals were
anesthetized using isoflurane (maintained at 1.5–2%), and Metacam (5 mg/kg) was given by
subcutaneous. One drop of 0.5% proparacaine hydrochloride ophthalmic anesthetic was instilled
prior to injection. The 30-gauge needle was inserted at an angle of 30° into the medial canthus,
and 1.4×10^{11} GC of the viral vector was delivered into the retro-orbital sinus. This method allowed
widespread brain expression of iGABASnFR2 in excitatory neurons for the optical detection of
extracellular GABA in mesoscale imaging studies.

Surgical procedure and electrophysiological recording setup

The animals were given buprenorphine (0.05–0.1 mg/kg, subcutaneously) 30 minutes prior to
surgery, and then isoflurane (1–2% oxygen) was administered via a nose cone. The scalp was
shaved and sterilized, and the skull was covered with C&B Metabond (Parkell, Inc.), to which a
custom-designed headplate was attached over the skull. A 12-mm glass coverslip (Carolina
Biological Supply, Cat. No. 633005) was then cemented to establish a chronic cranial window to
image at the mesoscale. The LFP recordings were obtained through teflon-coated 50 μm stainless
steel wires (A-M Systems) implanted for electrophysiology. A bipolar electrode was positioned in
the right hippocampus through craniotomy at approximately 2.6 mm laterally from the midline,
tangent to the posterior edge of the occipital suture. The electrode was advanced at a 57° angle
relative to vertical while monitoring neural signals both visually and audibly. Once optimal signal
quality was achieved, the electrode was fixed in place using Krazy Glue and C&B Metabond. In
addition, a bipolar EMG electrode was implanted in the nuchal muscles to record muscle tone.
LFP signals from hippocampal electrode was amplified (×1,000), bandpass filtered (0.1–10,000
Hz) using a Grass A.C. pre-amplifier (Model P511, Artisan Technology Group), and digitized at
20 kHz using a Digidata 1440 acquisition system (Molecular Devices Inc.).

Habituation for head-restraint sleep and wakefulness experiments

They were then gradually introduced to the recording device after 14 days of recovery by
positioning the animals on the recording platform. The first step consisted of letting the animals
get to the platform and adapt to the environment. On subsequent days, having settled, they were
positioned on head restraint in step increases in the period of head fixation, initiated at five minutes
during the first day and incremented in five-minute increases to a period of one hour total.

GABA imaging during wakefulness

Following the habituation, every animal was recorded every three days, with three to four sessions
being done on each mouse. The recording was always done at the same time of the day to reduce
variability and stress. Finally, the animals were put back into their home cages in the housing pod,
where they rested and recovered before the subsequent recording.

GABA imaging during natural sleep

Sleep recordings were performed after the completion of all wakefulness sessions. To optimize
conditions for natural sleep under head restraint, the day before recording, the animals were moved
from their home cage in the colony room to a separate room at noon. Sleep was restricted to ~6
hours by gently stimulating the mice with a cotton-tip stick whenever they showed signs of
drowsiness. The animals were then transferred to a larger cage containing new objects, such as a
running wheel, Cheerios, and a water container, and left in surgical recovery where the temperature
was controlled. The next day, the animals were transferred to the imaging room, and sleep
recordings began at ~7:00 AM. Once recording finished, the animals were returned to their home
cages in the podding room and allowed to sleep freely for at least three days before repeating the
procedure for another recording.

GABA imaging

Imaging was undertaken with a custom macroscope comprising a front-to-front video lens setup,
8.6×8.6 mm field of view. The focal plane was set ~0.5–1 mm below the cortical surface.
Fluorescence signals were recorded with a 12-bit CCD camera (1M60 Pantera, Dalsa, Waterloo,
ON) attached to an EPIX E8 frame grabber and operated by XCAP 3.8 software (EPIX, Inc.,

Buffalo Grove, IL), imaging at a frame rate of 80 Hz. Imaging parameters have been used in
previous studies, including voltage-sensitive dye imaging [25-27]. Sequential illumination was
provided using alternating blue (473 nm) and green (530 nm) LEDs (Thorlabs) [28]. Blue light (473
nm, filtered through a 467–499 nm bandpass) was employed to excite the iGABASnFR2 indicator,
and green light (530 nm, filtered through a 527/42 nm bandpass) for intrinsic signal imaging of
blood volume. A bandpass emission filter was placed in front of the CCD camera to facilitate
selective detection of either fluorescence or reflectance signals. Blue and green light-emitting
diodes (LEDs) were used as illumination sources. They were alternatively synchronized and
frame-by-frame, utilizing transistor–transitor logic (TTL) triggering, to offer temporal control
precisely so as to interleave acquisitions of reflectance and fluorescence images at 40 Hz per
channel. Reflectance images, which may be used for corrections of blood artifacts [29-31], were
analyzed as well within our current pipeline.

Preprocessing

Image data were transferred into MATLAB; blue and green frames were differentiated based on
reference frames to set up illumination origins. Only the region of interest (ROI) was selected
utilizing a binary mask. Slow baseline drifts were eliminated utilizing a local detrending algorithm,
based on a filter of the Chebyshev type. The ratio of $\Delta F/F_0$ was normalized to the fluorescence
signals (F) based on the following formula: $\Delta F/F_0 = (F - F_0) / F_0 \times 100$, where the detrended curve
provided an estimate of F_0. To filter out high frequency noise, a low-pass finite impulse response
(FIR) filter, utilizing a 6 Hz cut-off, was used on the time series of $\Delta F/F_0$. Hemodynamic artifacts
in the blue channel were corrected by linear regression, using the green reflectance signal as a
regressor. To denoise the data further, singular value decomposition (SVD) was applied to the
corrected blue channel, and the first 300 components were used for reconstruction.

Sleep scoring

Motion data were obtained from behavior camera (frame rate = 25HZ) by the FaceMap [32], which
computes frame-to-frame pixel intensity differences in manually defined regions of interest (ROIs).
Five ROIs—nose, whisker pad, ear, shoulder, and trunk—were selected to monitor both subtle
facial expressions and body movement. Motion signals were time-locked to electrophysiological
recordings. Wakefulness in this study was identified by clear motor activity in video recordings
and high EMG amplitude. NREM sleep was determined by decreased EMG tone, low hippocampal

theta-to-delta power ratio, and the occurrence of large irregular activity in the hippocampal LFP.
REM sleep was characterized by EMG suppression, sustained hippocampal theta oscillations, and
high theta-to-delta ratios.

SWR detection

SWRs were determined on the basis of a modified Karimi Abadchi et al [20] protocol. The raw LFP
signals of the hippocampus were initially down-sampled at 2 kHz and band-filtered between 110
to 250 Hz (ripple band) on a real-valued MATLAB (MathWorks) Morlet wavelet. The ripple-band
signal was then rectified and smoothed. screened SWRs were detected when ripple power crossed
above a threshold set as the mean plus a multiple of the standard deviation of the baseline. The
multiplier was set for each animal to compensate for inter-individual differences in signal quality.
Onset and offset times were set using a second threshold of 75% of the detection threshold. In
order to further refine event detection, only those SWRs with an appropriate duration were kept.
For each event window, event center was defined as the time of the greatest negative deflection
(trough) of the ripple-band sound. Events within 50 ms of an event were grouped into one SWR.

Normalization of peri-SWR neocortical activity using Z-scoring

To normalize peri-SWR neocortical GABA activity, random timestamps were created by
shufflings of the inter-SWR intervals within individual recording sessions. Imaging stacks 0.5
seconds before and 0.5 seconds after the timestamp were sampled and time-aligned for each
random event. Averaging peri-event stacks across all random timestamps were then calculated to
compute a baseline mean stack, as well as a parallel SD stack for standard deviation. These mean
and SD stacks served as references to z-score normalization. The peri-SWR imaging stacks were
then all normalized by subtraction of the baseline mean stack and division by the SD stack on a
pixel-by-pixel basis to provide a z-scored representation of neocortical activity.

Statistical Analysis

241   All statistical analyses were conducted using built-in functions in MATLAB.

Data availability

All data and custom software/algorithms necessary to interpret and replicate the findings and methods of this article are available upon request.

Results

Experimental protocol for investigating neocortical GABA dynamics

We retro-orbitally injected AAV2/PHP.N-Syn-Flex-iGABASnFR2 or control construct (cpSFGFP) into animals (see Figure 1A). The configuration of our recording involved mesoscale GABA imaging, in-vivo electrophysiological recordings, and monitoring of behavior (see Figure 1B). Protocols of imaging were conducted at 80 Hz cycling blue (470 nm) and green (530 nm) LEDs alternating with a CCD camera. LFPs were recorded from the right dorsal CA1 to study hippocampal sharp-wave ripples (SWRs), with neck EMG and a camera for monitoring behavior. A schematic of the headplate placement and the 17 cortical regions imaged in the right hemisphere is shown in **Figure 1Ci–ii**. Example cortical images are shown in Figure **1Ciii–iv**, with the dorsal retrosplenial cortex (dRSC) marked as a representative region of interest (ROI). To correct for hemodynamic artifacts, GABA fluorescence signals were normalized to simultaneously recorded reflectance traces (**Figure 1Cv–vi**).

Frames of images were registered to the center of SWR activity (see Figure 1Di), averaged and concatenated into single peri-ripple montages (see Figure 1Di–ii). To reveal cortical GABAergic inhibition dynamics, we provide two companion videos. **Video 1** provides spontaneous neocortical GABA dynamics during wakefulness, as $\Delta F/F_0$ signals via iGABASnFR2, together with hippocampal local field potential (LFP) and electromyography (EMG) traces verifying wakefulness. **Video 2** illustrates the multimodal sleep-scoring method, in combination of hippocampal ripple-band power, EMG power, raw EMG traces, pupil diameter, as verified in synchronized infrared video, to distinguish wakefulness, non-rapid eye movement (NREM) sleep, and rapid eye movement (REM) sleep.

Cortical GABA Dynamics Across Sleep-Wake State Transitions

To examine the spatiotemporal dynamics of neocortical GABA activity in state transitions, we unilaterally imaged fluorescence signals from the GABA-sensing reporter iGABASnFR2 by widefield imaging. Representative spatial montages and time series traces were analyzed to

evaluate GABA dynamics between cortical regions during transitions from NREM to wakefulness

and wakefulness to NREM sleep.

NREM to awake Transition

Figure 2Ai represents spatial montages of neocortical GABA activity at transition to wake (**Video**

3) with overall increases in fluorescence signal (z-scored ΔF/F) on transition, indicative of

increased levels of extracellular GABA. The phenomenon is quantified further in (**Figure 2Aii**),

which reveals regions such as V1, RSC2, and FLS1 exhibit a ramp-like build-up of GABA activity

begun several seconds before transition and peaking a short time after wake onset. **Figure S1iii**

validates the same in coherence spectra in increased inter-regional synchrony for delta and low-

theta bands on transition, and in functional connectivity (**Figure S2iv**), which similarly reveals a

transition from robust, spatially localized correlations in NREM to a global one in wake. The right-

most difference matrix reveals increased correlation of frontal and posterior cortices on transition.

Wake to NREM Transition

At wake-to-NREM transition (**Figure 2Bi**), spatial montages reveal a prominent reduction of

GABA fluorescence across the neocortex (**Video 4**). Time series traces in (**Figure 2Bii**) from the

same three areas exhibit a progressive decline in activity, starting approximately 5 seconds prior

to transition and persisting into early NREM. In parallel, **Figure S1i** reveals that there is increased

coherence in lower frequencies when entering NREM, pointing to more synchronous slow

oscillatory dynamics. Functional connectivity (**Figure S2iii**) confirms stronger localized

correlations in NREM relative to the more diffuse patterns of wake. The difference matrix reveals

increased correlation specifically in posterior and somatomotor areas.

NREM to REM Transition

Figure 3Ai depicts the spatial dynamics of GABA activity in NREM to REM transitions (**Video**

5). GABA activity seemed more spatially diverse than in other transitions, with some areas

showing transient increases and others remaining stable. Time series in **Figure 3Aii** indicate a

modest, transient increase in GABA levels in all three regions, followed by gradual suppression

throughout the REM episode. Coherence spectra in **Figure S1iv** show a decrease in inter-regional

synchrony in REM as compared to NREM. This is also reflected in the functional connectivity

heatmaps in **Figure S2ii**, which illustrate a general weakening of correlation patterns in REM. The

difference matrix indicates subtle reductions in cortical synchrony especially in posterior and
medial areas.

REM to Wake Transition

As illustrated in **Figure 3Bi**, the REM-to-wake transition (**Video 6**) is characterized by a trough
in GABA signal at the time of transition, followed by an abrupt rebound. The time courses of
Figure 3Bii indicate this transient inhibition most prominently in V1 and FLS1, and thus also
indicate a transient phase of disinhibition during transitioning out of REM. **Figure S1ii** indicates
wake-on transitions out of REM involve increases in coherence, particularly in delta and low-theta
frequencies, which would be consistent with reorganization into wakeful dynamics. Consistent
with this, the difference connectivity matrix of **Figure S2i** indicates heightened inter-regional
correlations following REM, particularly in anterior sensory-motor regions.

State-dependent spatiotemporal patterns of cortical inhibition around sharp-wave ripples

Studies have shown that sharp-wave ripples (SWRs) mediate communication between the
hippocampus and cortex in offline brain states, such as sleep and quiet wakefulness [33-37]. It has
been shown that the disruption of SWRs impairs memory consolidation, thus demonstrating their
functional importance [38-39]. These events represent an excellent portal for investigating localized,
temporally specific manipulation of cortical GABAergic inhibition. Following this background,
we next addressed the question of how neocortical GABAergic inhibition responds to SWRs
events. Using the iGABASnFR2 sensor, we combined unilateral imaging of neocortical
extracellular GABA with local field potential (LFP) recordings from CA1 pyramidal cells to study
the spatiotemporal features of extracellular GABA dynamics across the dorsal cortex in relation to
hippocampal sharp-wave ripples (SWRs) in natural sleep and wakefulness.

Montages of **Figure 4A**, reveal neocortical GABA's temporal and spatial pattern across different
states of the brain. Importantly, in time with NREM sleep (**Figure 4Ai**) neocortical GABA
activation began relatively early (**Video 7**), at approximately 150 ms before the SWR center (t =
0). The activation peaked in retrosplenial cortex (RSC) and occurred before the SWR center
(**Figure 4Bi**). The temporal profile of the activation was medial-to-lateral in direction, and medial
parts of the brain like the RSC exhibited earliest and greatest activation. Besides strong activation,
a clear GABA deactivation pattern was seen in lateral areas before the SWR center. These

observations lead us to speculate on the broader significance of GABAergic signaling in sleep and

wakefulness. Conversely, during wakefulness (**Figure 4Aii**), no initial GABA activation was

observed (**Video 8**). Rather, extracellular GABA activity within neocortical areas slowly built up

following the SWR center (t = 0), peaking ~ 500 ms after SWR (Figure 4Biii–iv).

Interestingly, wakefulness activation evolved in lateral-to-medial sequence, initiating in visual and

somatosensory cortices regions and spreading to medial regions. Deactivation of wakefulness was

much less strong and little suppression took place across regions before the SWR center, which

gave extra support to the state-dependent difference in the GABA modulation.

To explore the spatial organization of peri-SWR GABA activity in more depth, we examined four

major neocortical subnetworks: medial, visual, auditory, and somatomotor—as outlined in **Figure**

4Ci. Amplitude of activation were determined by taking mean of the complete signal in whole full

width at half-maximum (from t_1 to t_2), as in **Figure 4Cii**. Repeated measures ANOVA confirmed

sub-network-based effects for wakefulness and NREM. In wakefulness (**Figure 4Civ**), ANOVA

results showed significant subnetwork effect ($F(3,18) = 30.051$, $p = 3.18 \times 10^{-5}$; Greenhouse-

Geisser adjusted $p = 7.03 \times 10^{-5}$). Follow-up post-hoc analyses verified medial subnetwork had

highest activation amplitudes, which were higher comparing to auditory ($p = 0.0075$) and

somatomotor ($p = 0.0027$) subnetworks. The visual subnetwork had higher activation amplitudes

comparing to auditory ($p = 0.0025$) and somatomotor ($p = 0.0053$) subnetworks. Second, in NREM

(**Figure 4Cv**), the sub-network based effect attained significance ($F(3,12) = 21.608$, $p = 3.96 \times 10^{-5}$,

Greenhouse-Geisser adjusted $p = 0.0017$). Follow-up post-hoc analyses verified medial

subnetwork had highest activation, which was statistically significant comparing to auditory ($p = 0.0305$)

0.0305) and somatomotor ($p = 0.0366$) subnetworks. The visual subnetwork had intermediate

activation, and its amplitudes were higher comparing to auditory ($p = 0.0146$) and somatomotor

($p = 0.0366$) subnetworks.

Amplitudes of deactivation (**Figure 3D**) were explored and were found to exhibit state- and

specific patterns during wakefulness and NREM. During wakefulness (**Figure 4Di**), the

deactivations were attenuated but had robust subnetwork effects ($F(3,12) = 13.869$, $p = 0.00033$,

Greenhouse-Geisser adjusted $p = 0.0047$). The post-testing indicated that auditory subnetwork had

less deactivation compared to visual ($p = 0.032$) and medial ($p = 0.041$) subnetworks. The visual

subnetwork had greater deactivation than the somatomotor ($p = 0.061$) subnetwork. During NREM

(**Figure 4Dii**), deactivation amplitudes were significantly larger, with repeated measures ANOVA

indicating a strong subnetwork effect ($F(3,12) = 21.608$, $p = 3.96 \times 10^{-5}$; Greenhouse-Geisser

corrected p = 0.0017). Post hoc tests indicated significant differences between the auditory and visual (p = 0.015), auditory and medial (p = 0.031), and somatomotor and visual (p = 0.010) subnetworks.

To investigate state-dependent modulation more deeply, we recorded amplitudes of GABA activation and deactivation in different neocortical regions during wakefulness and sleep (**Figure S3A**). Activation and deactivation were comparable across states, as confirmed by correlation analyses (**Figure S3B**). Moreover, the comparisons of activation and deactivation amplitude at the subnetwork-specific levels discovered no statistically significant differences between NREM and wakefulness, again highlighting unique modulation profiles for both states (**Figure S3C**). **Activation Amplitudes:** A mixed repeated-measures ANOVA revealed a significant main effect of state on activation amplitudes ($F(1,10) = 28.266$, $p = 0.00034$), with NREM sleep exhibiting higher overall amplitudes. Subnetwork effects were also significant across states ($F(3,30) = 51.895$, $p = 5.50 \times 10^{-12}$), indicating robust differences among regions. However, the interaction between state and subnetwork was not significant ($F(3,30) = 1.605$, $p = 0.209$), suggesting that the relative differences among subnetworks were preserved across states. **Deactivation Amplitudes:** Similarly, for deactivation amplitudes, a mixed repeated-measures ANOVA showed a significant main effect of state ($F(1,8) = 18.571$, $p = 0.0026$), with NREM showing stronger deactivation than wakefulness. Subnetwork effects were again significant ($F(3,24) = 35.134$, $p = 6.08 \times 10^{-9}$), while the interaction between state and subnetwork was not significant ($F(3,24) = 1.686$, $p = 0.197$), indicating that subnetwork-specific patterns remained consistent across brain states.

Temporal mapping of cortical GABA peaks reveals brain-state-dependent propagation during SWRs

We then investigated the temporal profile of peak GABA activation across cortical areas. The time of peak neocortical GABA activation (t_p) was approximated, as the time of peak GABA signaling from the center of the SWR (**Figure 5Ai**), to measure the spatiotemporal extent of inhibition in SWRs in NREM sleep and wakefulness. t_p values in NREM sleep were highly regionally heterogeneous (**Figure 5Aii**), as confirmed by repeated-measures ANOVA ($F(10,40) = 5.0973$, $p = 8.91 \times 10^5$). Analysis of linear trends showed a weak but significant medial-to-lateral gradient in the time profile of activation (slope = 0.0113 s/region, $p = 0.047$). Spatial maps (**Figure 5Av**) showed the trend, with medial regions like RSC1 and RSC2 with earlier activation than the later

activation of lateral cortices. In wakefulness, t_p values had increased and more organized regional

heterogeneity (**Figure 5Aiii**), and signification effect confirmed by repeated-measures ANOVA

($F(10,60)$ = 20.156, p = 1.12×10^{15}). The linear trend discovered was stronger (slope =

0.0272 s/region, p = 0.024), and representative of a greater medial-to-lateral gradient.

Spatial maps (**Figure 5Avi**) confirmed this reversal of patterns: medial regions had later peak

GABA activation compared to lateral regions. Line-by-line comparison of trend slopes between

brain states (**Figure 5Aiv**) identified that the medial-to-lateral gradient was much greater during

wake than during NREM. In aggregate, these results define a state-dependent reorganization of

peak neocortical GABA timing: gradual and subtle during NREM sleep, but more sudden and

orderly during wakefulness. We compared rise times of extracellular GABA signals between

regions and states (**Figure S4A**). Rise times were similar in all cases, so variation in t_p found is

better ascribed to differences in timing, as opposed to in speed of activation. In addition, in

wakefulness,.t_p values were positively correlated (r = 0.558, p = 0.011; **Figure S4Bii**) with lateral

cortical location, as would be expected for a lateral-to- medial propagation of GABA activation.

In NREM sleep, however, there was a significant negative correlation (r = –0.391, p = 0.040;

Figure S4Biii), indicative of medial regions' earlier activation. These results lend further support

to a state-dependent reorganization of spatiotemporal characteristics of neocortical GABAergic

signaling during hippocampal SWRs.

Spatial and temporal modes of peri-ripple iGABASnFR2 activity and region-specific

dynamics

We then examined if ripple-related neocortical GABA dynamics show unique spatial motifs and

temporal structures at the network level. To decompose spatiotemporal neocortical GABA activity

into general spatial and temporal structures, we applied singular value decomposition (SVD) to

GABA signals close to SWRs **(Figure 6A, B)**. Component 1 mapped diffuse activation of GABA

(Components 1i), and the corresponding temporal trace (Component 1ii) consisted of a punctuate

onset of extracellular GABA at ripple onset (t = 0). Components 2–5, on the other hand, detected

state-specific characteristics. In wakefulness (**Figure 6A**), spatial maps (Components 2–5i)

illustrated regionally localized activation of GABA in lateral regions, but corresponding temporal

traces (Components 2–5ii) contained transient, fast features, suggesting fast, region-specific

inhibition. In NREM sleep (**Figure 6B**), higher-order spatial components detected heightened

recruitment of medial regions, including the retrosplenial cortex (RSC). The temporal components in NREM were slow and less well time-locked to onset of ripples compared to wakefulness. We also reconstructed neocortical GABA activity in the neocortex close to SWRs in five representative neocortical locations: RSC, BC, V1, auditory cortex (AUD), and forelimb somatosensory cortex (FLS1) (**Figure 6C, D**). Under wakefulness (**Figure 6C**), BC and V1 had sharp, high-amplitude GABA transients (**Figure 6Cii**), and statistical comparisons revealed heightened GABA responses in sensory areas compared to the RSC (**Figure 6Ciii**). During NREM sleep (**Figure 6D**), RSC has the strongest activation (**Figure 6Dii–iii**). Combined, these results show that while a global elevation of inhibitory tone accompanies hippocampal ripples in both brain states, fine-scale spatiotemporal patterns of neocortical GABA dynamics depend on brain state. Wakefulness involves rapid, GABA activation in lateral sensory cortices, while NREM sleep recruits more widespread, slower inhibitory responses with a focus on medial areas.

Discussion

Summary of the Study

In this study, we investigated how neocortical GABAergic inhibition is temporally and spatially organized around internally generated hippocampal sharp-wave ripples (SWRs) across behavioral states. Using mesoscale imaging of extracellular GABA with the iGABASnFR2 sensor alongside simultaneous recordings of CA1 pyramidal neuron activity, we first characterized GABAergic activity during spontaneous transitions between sleep and wakefulness. Next, we explored spatiotemporal dynamics of neocortical GABA around hippocampal SWRs and found that cortical GABAergic inhibition is spatially structured, exhibits propagating dynamics, and is strongly modulated by brain state. Our results revealed distinct patterns of neocortical GABA dynamics around SWRs , with medial-to-lateral propagation during NREM sleep and lateral-to-medial propagation during wakefulness. Our results suggest that cortical GABAergic inhibition is actively modulated by hippocampal output, and that this modulation differs across cortical subnetworks and vigilance states.

To examine how GABAergic inhibition in the cortex is regulated by hippocampal sharp-wave ripples (SWRs), we employed the genetically encoded GABA sensor iGABASnFR2, allowing direct optical imaging of extracellular GABA dynamics in vivo [21]. We wanted to quantify GABAergic inhibition across the whole dorsal cortex and thus conducted widefield imaging

through a large cranial window over the right hemisphere. To record hippocampal output in parallel, we measured local field potentials from the ipsilateral dorsal hippocampus. This unilateral approach was informed by previous reports of strong interhemispheric synchrony in both neocortical activity [40] and hippocampal SWRs [33,37], which made it adequate to describe ripple-cortical interactions. This setup enabled us to integrate mesoscale imaging with exact electrophysiological timing to investigate inhibitory dynamics during natural sleep and wakefulness at high spatial and temporal resolution.

Cortical GABA Dynamics During State transitions

First, we examined the changes in cortical GABA levels that take place during spontaneous behavior state transitions, and we complemented this analysis with coherence and correlation-based network methods to reveal their implications at the circuit level. As the brain transitioned from NREM sleep to wakefulness, we observed a dramatic increase in GABA activity, which was replicated across different cortical areas (**Figure 2Ai–ii**), and increased inter-areal coherence and functional connectivity (**Figures S1iii, S2iv**). This increase in inhibitory tone, coupled with increased synchrony, can reflect an active gating or stabilization process during the arousal process, promoting the coordination of sensory and motor pathways as the brain prepares for the state of behavioral responsiveness [41-43]. In contrast, transitions from wakefulness to NREM sleep were correlated with a decrease in extracellular GABA (**Figure 2Bi–ii**), together with increases in slow-frequency coherence (**Figure S1i**) and more tightly localized functional correlations (Figure S2iii). These are likely to represent a switch from fast, phasic inhibitory mechanisms to slower, synchronous, oscillatory modes typical of NREM sleep [44-45], in favor of the commencement of cortical downscaling and memory consolidation.

The dynamics of GABA in the neocortex across transitions involving REM sleep showed increasingly complex and varied dynamics. The transition from NREM to REM sleep was marked by modest, regionally specific increases in GABA levels, which were then followed by suppression (**Figure 3Ai–ii**). This transition also showed a decrease in coherence and weakening of inter-areal correlations (**Figures S1iv, S2ii**), consistent with the decoupled cortical dynamics characteristic of REM sleep. In contrast, the transition from REM sleep to wakefulness showed a large drop in GABA at the point of awakening (**Figure 3Bi–ii**), followed by rapid re-engagement, reflecting a brief release from inhibitory control [46-49]. This transition was accompanied by a large increase in coherence and correlation strength (**Figures S1ii, S2i**), marking a reorganization of network

synchrony required for cognitive and sensory engagement in wakefulness. Together, these findings
highlight the dynamic and state-specific regulation of GABAergic tone across the neocortex,
indicating that changes in inhibitory signaling are closely intertwined with macroscale network
reconfiguration across sleep-wake transitions.

Ripple-triggered GABA responses are brain-state dependent

Past research with iGluSnFR has established that hippocampal SWRs are coordinated by state-
dependent cortical excitation [19-20]. Our results build on this research by demonstrating that cortical
inhibition, as assayed by the extracellular GABA imaging, is also state-dependently coordinated
on SWRs. During NREM sleep, we found that extracellular GABA levels increased starting before
ripple onset in medial cortical areas, including the retrosplenial cortex. This result is consistent
with past work showing that SWRs recruit retrosplenial inhibitory neurons to fire during slow-
wave sleep 50 and aligns with prior research on retrosplenial–hippocampal coordination during
memory-related processing [51-52]. This initial medial activation was joined by a simultaneous
deactivation in lateral sensory cortices, implicating a topographically organized inhibition pattern.
By contrast, during wakefulness, GABAergic activity increased in primarily lateral cortical areas
after ripple onset, whereas medial areas showed delayed or reduced responses. These findings
together demonstrate that SWRs recruit not just excitatory but also inhibitory cortical networks in
a temporally and spatially coordinated fashion, and that the organization of this recruitment is
radically different in sleep versus wakefulness.

Temporal gradients reveal propagation of inhibitory signals

Time-to-peak (t_p) of neocortical GABA dynamics throughout different cortical areas showed
medial-to-lateral propagation during NREM sleep, consistent with glutamate dynamics [19] and
memory-related information flow direction between default-mode network structures. During
wakefulness, direction of propagation was reversed, and propagation went from lateral to medial
cortical compartments. These results are in concert with the suggestion that cortical inhibition
characteristically follows excitation with a characteristic temporal delay [1,53,54] Neocortical
inhibition in this case can function as a state-dependent gate of the hippocampal output,
orchestrating temporally the inhibition control with the current sensory or cognitive demands.
Directional asymmetry of propagation patterns uncovers the cortex to rescale not only the strength
but also the spatiotemporal organization of inhibition in accordance with internal state.

SVD reveals global vs. local components of ripple-evoked inhibition

Our SVD characterization of neocortical GABA signals in hippocampal SWRs revealed typical
spatial and temporal patterns of inhibition. The first factor described a global increase in GABA
activity throughout the cortex that could be a generalized and synchronized inhibitory response
potentially used to suppress cortical excitability and runaway excitation in the progression of
memory-related hippocampal activity. Beyond this, components 2-5 represented more localized
and state-dependent dynamics. When awake, these components identified fast, transient increases
in GABA activity in mostly lateral cortical regions, which may represent regionally selective
gating of sensory information or circuit inhibition. During NREM sleep, GABA activity exhibited
wider and more sustained increases in medial regions, including the RSC, a region highly
interconnected with the hippocampus and involved in memory consolidation processes [35,46]. These
results indicate that SWR-evoked GABAergic inhibition is not homogeneous throughout the
cortex but rather consists of a global inhibitory scaffold with overlaid state-specific, spatially
directed components that can facilitate the routing and integration of memory-related information
during sleep and wakefulness.

Conclusion

In the current study, mesoscale imaging of iGABASnFR2 was used to map the dynamics of
extracellular GABA over the dorsal cortex during sleep-wake transitions and in response to
hippocampal sharp-wave ripples. The results show that cortical GABAergic inhibition is spatially
patterned and under strong control of behavioral states, suggesting that neocortical GABA
dynamics play an active role in the routing and filtering of memory-related outputs from the
hippocampus. While our imaging approach provides high temporal and spatial resolution over
large cortical areas, it remains nonspecific with regard to cell types and depth resolution. Therefore,
it would not be possible to distinguish between the behaviors of PV+, SST+, or VIP+ interneurons,
or clarify the inhibitory roles at the subcortical level. To further define the circuit mechanisms
underlying state-dependent and ripple-dependent inhibition, future studies employing
iGABASnFR2 in conjunction with optogenetic manipulation, cell-type-specific marker labeling,
or multiphoton microscopy will be necessary. In addition With recent advances in genetically
encoded sensors, it is now possible to simultaneously measure excitation and inhibition in vivo.

Combining iGABASnFR2 with glutamate sensors will enable direct assessment of excitation–
inhibition balance in both healthy and disease models, offering new insights into how this balance
is altered in disorders such as epilepsy or schizophrenia.

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Author contributions

559 E.R. conceptualized the study, and E.R. performed the experiments. E.R. and S.T. analyzed the
560 data. E.R. wrote the manuscript and prepared figures.

Competing interests

562 The authors declare no competing interests.

Supplementary material

564 Supplementary material and methods are available .

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Figure legends

Figure 1. Experimental protocol for imaging neocortical GABA dynamics during sleep and hippocampal ripples. (A) Schematic of viral delivery and genetic targeting. Emx1-Cre mice received retro-orbital injections of either AAV2/PHP.eB-Syn-Flex-iGABASnFR2 or AAV2/PHP.eB-Syn-Flex-cpSFGFP as a control. In Emx1-Cre mice, Cre recombinase drives expression of the GABA sensor iGABASnFR2 or control construct specifically in cortical excitatory neurons. iGABASnFR2 is membrane-bound and reports extracellular GABA binding

via fluorescence increases, whereas cpSFGFP is cytosolic and does not respond to GABA. (B) Diagram of the in vivo imaging and recording setup. A CCD camera captures widefield fluorescence from the dorsal cortex through a cranial window. Imaging is synchronized to alternating blue (470 nm) and green (530 nm) LED strobes at 80 Hz for excitation of iGABASnFR2 and collection of reflectance signals, respectively. Simultaneous recordings include hippocampal LFPs from dorsal CA1 to detect SWRs, neck EMG for movement and arousal state, and a behavioral camera (25 Hz) for motion tracking via FaceMap. (C) Imaging coverage and signal correction. (i)Schematic showing the imaging configuration: the right hemisphere was exposed for imaging which was sealed it with Metabond, while the left hemisphere remained intact. (ii) Schematic showing the 17 identified cortical regions used in ROI-based analyses. (iii–iv) Example cortical images under blue and green LED illumination. The red box marks the dorsal retrosplenial cortex (dRSC), one of the key analysis regions. (v) Traces from the same site showing raw iGABASnFR2 fluorescence (blue), reflectance (green), and the hemodynamically corrected signal (black). (vi) Example traces showing simultaneous hippocampal LFPs (broadband and ripple-filtered), local dRSC LFP, and corrected GABA fluorescence from dRSC. Detected SWRs are aligned with both GABA and LFP signals. (D) Alignment and averaging of peri-ripple GABA activity. (i) Example SWRs from the ripple-band filtered LFP (100–250 Hz) are aligned with concurrent widefield GABA imaging frames. (ii) For each detected SWR, peri-event GABA imaging frames are extracted, aligned to the ripple center (t = 0), and assembled into individual montages. Mean peri-ripple maps are generated across events to characterize spatiotemporal GABA dynamics around SWRs.

Figure 2. Neocortical GABA activity during NREM is used to awaken and awaken NREM transitions. (A) Transition from NREM to Awake. (i) Representative montage of mean neocortical GABA activity during wake-NREM transition recorded with the GABA-sensing fluorescent reporter iGABASnFR2. Images present 5-second time bins, and zero s-time marks wake onset. Data were scaled and z-scored to the shown color bars (n=5). (ii) Representative

sample traces of iGABASnFR2 signals from regions indicated in (i). The plots present the mean
optical signals recorded in 3×3-pixel boxes (~ 0.04 mm^2) throughout cortical regions. Width of
shading surrounding each plot indicates standard error of the mean (SEM). The time 0 s indicates
wake onset. (B) Transition from Awake to NREM. (i) Representative montage of mean neocortical
GABA activity during wake-NREM transition. Images present 5-second time bins, and zero s-time
marks NREM onset. Data were scaled and z-scored to the shown color bars (n=5). (ii)
Representative sample traces of iGABASnFR2 signals from regions indicated in (i). The plots
present the mean optical signals recorded in 3×3-pixel boxes (~ 0.04 mm^2) throughout cortical
regions. Shaded areas surrounding each trace indicate reproducibility, which is confirmed. The
time 0 s indicates NREM sleep onset.

Figure 3. Neocortical GABA Activity During NREM to REM and REM to Awake Transitions. (A) Transition to REM. (i) Montage of mean neocortical GABA activity recorded using the GABA-sensing fluorescent reporter iGABASnFR2 during natural sleep. Images represent 5-second epochs, and zero s-time represents REM onset. Data were z-scored and normalized to the color bars shown (n=5). (ii) Representative traces of iGABASnFR2 signals from regions marked in (i) in an exemplary animal. The plots show the mean optical signals recorded in 3 × 3-pixel boxes (~0.04 mm²) within the visual (V1), retrosplenial (RSC), and forelimb

somatosensory (FLS1; magenta) cortices. The thickness of the shading around each plot gives the
SEM. The time 0 s represents REM onset. (B) Transition to wake at wake-onset. (i) Montage of
mean neocortical GABA activity recorded using the GABA-sensing fluorescent reporter
iGABASnFR2 during wake-onset transition from REM. Images represent 5-second epochs, and
zero s-time represents wake-onset. Data were z-scored and normalized to the color bars shown
(n=5). (ii) Representative traces of iGABASnFR2 signals from regions marked in (i) in an
exemplary animal. The plots show the mean optical signals recorded in 3×3-pixel boxes (~0.04
mm^2) within the visual (V1), retrosplenial (RSC2), and forelimb somatosensory (FLS1; magenta)
cortices. The thickness of the shading around each plot gives the SEM. The time 0 s represents
wake-onset.

Figure 4. Peri-SWR neocortical GABA activity: activation and deactivation patterns across
sleep and wake states. (A) Characteristic montage of mean peri-SWR neocortical GABA activity,

as visualized with the GABA-sensing fluorescent reporter iGABASnFR2, during head-restrained
natural sleep (i) and wakefulness (ii). Time 0 marks SWR centers. Images z-scored and scaled to
respective color bars. (B) (i–iv) Sample traces of iGABASnFR2 signals. Panels (Bi, Bii) show
natural sleep traces, and (Biii, Biv) show wake traces, taken from sample regions in panels (Ai)
and (Aii). Traces show mean optical signals from 3×3-pixel boxes (~0.04 mm²) within
retrosplenial (blue), visual (black), and forelimb somatosensory (magenta) cortices. Shaded areas
around regions of each plot are SEM. SWR centers mark time 0. (C) (i) Four large neocortical
subnetworks (medial, visual, auditory, and somatomotor), structurally delimited. (ii)
Quantification of activation amplitude schema, defined as mean within-whole-width-at-half-
maximum (t1 to t2) of the mean. (iv–v) Grand average (n = 7 animals) of activation amplitudes
across subnetworks during wake and sleep, ordered in decreasing order. Each data point represents
average activation amplitude for all regions within a subnetwork for one animal. Statistical
Analysis: Awake data had a significant subnetwork influence ($F(3,18) = 30.051$, $p = 3.18 \times 10^{-7}$,
Greenhouse-Geisser adjusted $p = 7.03 \times 10^{-5}$), and post-hoc differences were found between
auditory and medial ($p = 0.0075$), auditory and visual ($p = 0.0025$), medial and somatomotor ($p =$
0.0027), and somatomotor and visual ($p = 0.0053$). Sleep data also revealed a significant
subnetwork effect ($F (3,12) = 21.608$, $p = 3.96 \times 10^{-5}$, Greenhouse-Geisser corrected $p = 0.0017$),
with posthoc differences between auditory and medial ($p = 0.0305$), auditory and visual ($p =$
0.0146), and medial and somatomotor ($p = 0.0366$). (D) (i–iii) neocortical deactivations preceding
SWRs. (Di, Dii) show results for wakefulness and sleep, respectively. Deactivation amplitudes
were rectified for group comparison, with higher values indicating more substantial deactivation.
Bar plots depict mean ± SEM. Statistical Analysis: Awake data recorded a significant subnetwork
effect ($F (3,12) = 13.869$, $p = 0.00033$, Greenhouse-Geisser corrected $p = 0.0047$), and posthoc
differences between auditory and visual ($p = 0.032$), medial and somatomotor ($p = 0.041$), and
visual and somatomotor ($p = 0.061$) regions. Sleep data recorded a significant subnetwork effect
($F (3,12) = 21.608$, $p = 3.96 \times 10^{-5}$, Greenhouse-Geisser corrected $p = 0.0017$), and posthoc
differences between auditory and visual ($p = 0.015$), auditory and medial ($p = 0.031$), and
somatomotor and visual ($p = 0.010$) regions. There are five supplementary panels in the figure.

Figure 5. Cortical regions exhibit state-dependent peak GABA activation dynamics around SWRs during natural sleep and wakefulness. (A) (i) Peak GABA activation time (tp) for peri-SWR in each cortical region was determined as peak time of mean peri-SWR GABA activity trace (blue trace) and provides an index of peak GABA activation time relative to center of SWR. (ii) Sleep Condition: Repeated-measures ANOVA revealed significant regional variation in tp $(F(10,40) =5.0973, p=8.9111e{-}05)$. A statistically significant positive linear trend (slope=0.011273 s/region,p=0.047249) discloses medial-to-lateral progression of tp during sleep, consistent with a subtle medial-to-lateral propagation of GABA activation. (iii) Awake Condition: Repeated-measures ANOVA revealed strong and statistically significant regional variation in tp $(F(10,60) =20.156, p=1.116e{-}15)$. Post-hoc linear trend analysis confirmed a statistically significant positive slope (slope=0.02724 s/region, p=0.024326), which discloses a consistent and systemicdelayed,tp from medial toward lateral regions in wake stage. (iv) Post-hoc Linear Trend Analysis: Linear trend analysis confirmed state-dependent dynamics. In wake, a statistically significant positive slope (0.02724 s/region=0.024326) discloses a robust medial-to-lateral gradient. In sleep, a negligibly but statistically significant smaller slope (0.011273 s/region=0.047249) reveals less strenuous regional variations. The corresponding graph reveals the result, which shows steep and consistent regional variation in awake data compared with sleep. (v) Spatial maps during sleep (n=5) reveal higher earlier peak tp in medial regions like RSC1, RSC2, and PtA, and subsequent lateral propagation of activation. The result discloses an orchestrated medial-to-lateral propagation of GABAergic activation during natural sleep. (vi) Spatial maps for wakefulness (n=7) indicate delayed activation in medial regions and a more homogeneous distribution of tp values throughout cortical regions. The pattern indicates characteristic cortical dynamics in wakefulness, with a strong medial-to-lateral gradient in GABA activation timing.

Figure 6. Spatial and Temporal Modes of Peri-Ripple iGABASnFR2 Activity and Region-Specific Dynamics. (A, B) Spatial (i) and temporal (ii) modes of the five largest singular components of the peri-ripple combined iGABASnFR2 activity stack in wakeful (A) and sleep (B) epochs. Spatial mode of first component exhibits absence of sharp topographical features, consistent with a widespread increase of the iGABASnFR2 signal following the ripple, which overwhelms the entire GABA signal and corresponding temporal mode. This overall response is invariant across states, with the temporal amplitude of the first component being one order of magnitude larger than the others, thus revealing its predominance in describing the dynamics of global peri-ripple GABA activity.Components 2–5 demonstrate state-dependent differences in the spatiotemporal structure of GABA activity. When awake (A), spatial maps of Components 2–5 illustrate localized GABA activity, with particularly strong activity in sensory areas like the barrel cortex (BC) and visual cortex (V1). Their temporal profiles reveal rapid, sharp peaks at fixed times of ripple initiation, which can be resolved as specific and region-specific GABAergic control. Asleep (B), spatial modes of Components 2–5 reveal less spatially localized patterns of increased associative area activity (e.g., retrosplenial cortex, RSC) and decreased sensory area activity—corresponding temporal profiles asleep reveal slower dynamics, and bear no such sharp peaks as during wakefulness. (C, D) Peri-ripple regional GABA activity reconstructed for significant regions of interest (ROIs)—the retrosplenial cortex (RSC), barrel cortex (BC), visual cortex (V1), auditory cortex (AUD), and forelimb somatosensory cortex (FLS1)—reveal state-dependent peri-ripple dynamics. These findings have considerable implications for our understanding of brain activity in wakefulness and sleep. Awake (C), BC and V1 reveal well-defined and high-amplitude peaks in their temporal profiles (Cii), and statistical comparison (Ciii) reveals significantly increased sensory responses as compared to RSC. When asleep (D), GABA activity is more diffusely distributed across areas, with RSC standing out as the predominant area with prolonged and sizable activity. Sensory areas like BC and V1 have weakened responses when asleep (Dii). Shading in temporal profiles (Cii, Dii) denotes the SEM and statistical comparison (Diii) emphasizes the relative enhancement of RSC activity with respect to sensory areas when asleep. Shading around these profiles also denotes the SEM.