Synaptic high-frequency jumping synchronises vision to high-speed behaviour

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Abstract

During high-speed behaviour, animals must predict, detect, process, and respond synchronously to rapid environmental changes, including those caused by their own movements. How neural systems achieve such precision remains unclear. Here, we investigate how the housefly (*Musca domestica*), renowned for agile aerial manoeuvres, maintains visual accuracy during ultrafast motion. Although rapid movements typically blur vision, houseflies exhibit remarkable visual acuity; their visual neurons achieve record-high rates of information sampling (~2,500 bits/s) and synaptic transmission (~4,100 bits/s), substantially surpassing previous estimates. Using intracellular and photomechanical recordings of photoreceptors exposed to rapid sequences of saccade-like stimuli, we traced information transmission to large monopolar cells (LMCs), the first interneurons in the visual pathway. We identify a previously unknown mechanism—*synaptic high-frequency jumping*—in which photoreceptor–LMC synapses dynamically shift transmission towards higher frequencies during saccadic input. This mechanism extends visual bandwidth to ~920 Hz, eliminates synaptic delays, and quadruples traditional flicker-fusion limits (~230 Hz). Ultrafast behavioural experiments confirm flies respond synchronously within ~13–20 ms, even while photoreceptor responses are still

approaching their peak (9–16 ms), directly challenging classical sequential-processing models. Our biophysically realistic photoreceptor–LMC model demonstrates how photomechanical, quantal, and refractory sampling processes co-adapt dynamically with behaviour. Thus, flies actively shape their visual input through self-generated saccades, driving high-frequency jumping, efficient neural coding, hyperacute vision, and neural synchronisation. These findings redefine foundational principles of compound-eye function, uncovering a universal neural strategy underlying synchronous, high-speed predictive processing.

Main

Animals moving at high speeds must process visual information rapidly to avoid motion blur. How neural circuits achieve this—and whether self-motion helps or hinders perception—remains unclear. Answering this requires examining how innate and learned behaviours refine sensory perception to support survival. Brains, constrained by thermodynamics, genetics, and cellular biophysics, dynamically harness electrochemical, kinetic, and thermal energy to respond rapidly and accurately to internal and external signals[1]. Yet prevailing models often oversimplify neural signalling by treating neurons as static, unidirectional transmitters, neglecting the role of rapid physical movements at the ultrastructural level[2-8]. Such *morphodynamic interactions*—ultrafast, activity-dependent mechanical and structural changes in neural elements—include photoreceptor microsaccades[1,2,9-15], quantal neurotransmitter release[6,7,14-16], and synaptic feedback mechanisms[17-20]. These phenomena collectively accelerate and enhance neural signalling, enabling rapid and precise perception and action[11,16].

Houseflies exemplify extraordinary aerial agility[21], suggesting exceptional visual capabilities shaped by strong evolutionary pressures[22]. Historically, however, flies were presumed incapable of resolving fine visual details during rapid movements. Fast body and head movements (saccades) produce high angular velocities[21,23-26], which, coupled with presumedly slow photoreceptor responses, were thought to blur vision[27,28]. Although compensatory head and thorax adjustments[25,26,29,30] and specialised retinal zones[31,32] partially mitigate this blur, rapid saccades were still assumed to momentarily render flies "blind"[33]. Yet this longstanding assumption contradicts flies' remarkable ability to evade threats: how could flies buzzing around your head in summer, effortlessly dodging every swat, truly have impaired vision?

To address this paradox, we examine neural responses using controlled saccadic stimuli—light patterns effectively mimicking the temporal characteristics of natural saccades—to isolate visual processing from voluntary flight complexities. We hypothesise that the fly's visual system has evolved specifically to process rapid saccadic inputs with exceptional speed, accuracy, minimal latency and noise. Using intracellular recordings, photoreceptor microsaccade measurements,

ultrastructural analyses, and a biophysically realistic computational model of the *morphodynamic neural superposition system*[1,11,34] (**Figure 1**), we investigate how photoreceptors and large monopolar cells (LMCs) dynamically sample and encode visual information. We specifically explore how neural structure–function relationships have co-evolved with saccadic behaviour to maximise coding efficiency. By comparing empirical data and simulations of photoreceptor-LMC interactions within a novel theoretical framework—morphodynamic information processing[1]—we identify and mechanistically explain a new phenomenon—synaptic high-frequency jumping—arising from coordinated morphodynamic sampling of rapid saccadic light changes, which enables hyperacute predictive vision.

Multiscale Experimental Analysis

Experimentally, we assessed the compound eyes' signalling performance by studying both static and dynamic properties (**Figure 1a**; **Supplementary Information, Sections I-III**). To examine static structure, we used synchrotron X-ray imaging (**i**) and electron microscopy (**ii**) on fixed preparations to characterise the optical and ultrastructural adaptations. This included measuring the size and positioning of R1–R6 rhabdomeres across the eye and quantifying how many microvilli—photon-sampling units—each photoreceptor contains.

To assess dynamic properties, we investigated neural morphodynamics in intact living flies. Using high-speed infrared microscopy (**iii**), we recorded photomechanical microsaccades within neighbouring ommatidia (**iv**), and applied beam-propagation modelling[11] (**v**) to estimate how these microsaccades move and narrow R1–R6 receptive fields locally. Finally, we used sharp microelectrodes (**vi**) inserted through a small corneal opening to record intracellular voltage responses of photoreceptors and LMCs to light stimuli.

Figure 1. Investigating morphodynamic neural superposition system in the housefly compound eye.
(**a**) Key structural and functional components underlying the housefly's morphodynamic vision were studied using both static imaging and live-recording approaches.
(**i**) The optical architecture of ommatidial structures was analysed in fixed eyes using synchrotron X-ray imaging.

(**ii**) The number of independent photon-sampling units (microvilli) in R1–R6 photoreceptor rhabdomeres was estimated via electron microscopy.
(**iii**) High-speed infrared optical imaging enabled in vivo tracking of photoreceptor movements in response to light flashes.
(**iv**) These recordings revealed photomechanical microsaccades—small, directionally diverse shifts of photoreceptors within ommatidia.
(**v**) Microsaccades shift photoreceptor receptive fields (RFs; circles), which overlap to tile the compound eye's visual field in an overcomplete pattern[11,34]—i.e., overlapping but not perfectly aligned, unlike earlier assumptions[35,36]. Each local LMC's receptive field combines the photomechanically moving RFs of R1–R6 within a morphodynamic neural superposition system.
(**vi**) Intracellular voltage responses of photoreceptors and large monopolar cells (LMCs) to light stimuli were recorded using sharp microelectrodes.
(**b**) Representative experimental responses to a 10 ms UV flash (green bar): submicrometre photomechanical microsaccades (top), rapid voltage changes in photoreceptors (middle), and downstream LMCs (bottom). R1–R6 photoreceptors in neighbouring ommatidia sample the scene independently, producing variable phase-shifted voltage responses (spatiotemporally overcomplete sampling of the light stimulus) that converge onto a shared LMC, generating a morphodynamically shaped, transient voltage response (thin traces = individual responses, thick traces = mean responses).
(**c**) Simulated responses from a biophysically realistic model of the morphodynamic neural superposition system, in which over-completely tiled photomechanically moving photoreceptor receptive fields[11,34], replicate the observed microsaccades and voltage responses. Informed by anatomical and physiological measurements in (**a**), the model accurately predicts receptive field movements and signal propagation through the photoreceptor–LMC circuit.

Biophysical Model of Morphodynamic Encoding

We used experimental findings to construct a biophysically accurate multiscale model of the R1-R6 photoreceptor–LMC network (**Figure 1c**; **Supplementary Information, Section IV**). Beneath each ommatidial lens, each modelled photoreceptor sampled photon rate changes from its realistic receptive field via photomechanical movements[2,9,11]—rapidly contracting and elongating along its optical axis while shifting laterally in a complex piston-like motion. These microsaccades continuously reshaped and repositioned receptive fields in response to visual stimuli, depending on the size, eccentricity, and motion axis of each photoreceptor's light-sensing structure, the rhabdome. Each R1–R6 rhabdomere contains a distinct number of microvilli—ranging from ~41,000 to ~74,000 depending on eye location (see **Supplementary Information, Section II**)—each functioning as an individual photon-sampling unit[37]. The model generated macroscopic R1–R6 photoreceptor responses from quantal photon absorptions and integrated these dynamic inputs through feedforward and feedback synapses to form a *morphodynamic neural superposition system* that continuously adapted the information flow between photoreceptors and LMCs to maximise visual encoding.

In the real eye, thousands of these morphodynamic neural superposition units tile the visual surface, forming overcomplete, localised encoding channels (**Figures 1a**-iv, v and **1b**). Our model replicates how these units sample and process quantal visual information—i.e., changes in photon absorption rate—without requiring adjustable parameters. This framework links neural morphodynamics[1,9,11] and active sampling dynamics[38-40] to emergent coding strategies, such as network synchronisation, that enable high-speed vision and visually guided behaviour.

Saccadic Bursts Amplify Neural Signalling

We performed electrophysiological experiments (**Figure 2a**) using 'saccadic' light stimuli, which mimic the rapidly changing intensity patterns experienced by photoreceptors during natural visual behaviours. These stimuli featured rapid contrast fluctuations—ranging from moderate (c ≈ 0.6) to high (c ≈ 1.5)—across multiple temporal frequencies (20, 50, 100, 200, and 500 Hz; **Figure 2b**). As a control and to benchmark our findings against classical studies[41-45], we also applied low-contrast (c ≈ 0.3), bandwidth-limited Gaussian white noise (GWN) stimuli (**Figure 2c**).

GWN stimuli, traditionally used for estimating neural information capacity[41-45], are known to reduce encoding efficiency in neurons such as photoreceptors[9,46-49] and LMCs[16], which integrate quantal events (e.g., photon and neurotransmitter arrivals) through refractory sampling[9,46,47]. Each photoreceptor microvillus—a discrete photon-sampling unit—generates a quantum bump only after fully recovering from its previous phototransduction event[46,47,50]. Because GWN lacks the temporal structure of natural stimuli, it drives these sampling units into prolonged refractory states, impairing ability to track rapid photon-rate changes, and thereby reducing response amplitude and information content[9,46,47,51].

Consistent with this, photoreceptors and LMCs exhibited their strongest responses to high-contrast saccadic bursts (**Figure 2c**). These stimuli comprise brief, bright events separated by short, darker intervals, which allow photoreceptors to recover from refractoriness and integrate more photon quanta efficiently[9]. In contrast, responses to low-contrast GWN stimuli were significantly smaller and decreased further as stimulus frequency increased (bottom row, right column). The 500 Hz GWN stimulus was particularly ineffective, revealing a limit in how well these neurons can track rapidly changing, randomly ordered light contrast changes.

Figure 2. Synaptic high-frequency jumping in the morphodynamic neural superposition system: shifting saccadic light information from photoreceptors to higher-frequency band in LMCs.
(**a**) Left-schematic: The Cardan arm system positions light-point stimulus (L) at the centre of the recorded neuron's receptive field, while micromanipulator-controlled measurement (M) and reference (R) microelectrodes record intracellular voltage responses. Right-schematic: R1-R6 photoreceptor and LMC recordings are conducted separately from the retina and lamina of intact, head-fixed flies (with intact eyes, red in the inset).

(**b**) Typical photoreceptor and LMC voltage responses to 30 repetitions of 2-second-long 100 Hz high-contrast bursts.

(**c**) Photoreceptor and LMC responses to varying stimuli, from high-contrast "saccadic" bursts to low-contrast Gaussian white-noise (GWN) stimuli across specific bandwidths (20, 50, 100, 200 and 500 Hz). Mean (thick traces) and individual responses (thin) to repeated stimuli (coloured). The yellow box highlights the most varying responses to 100 Hz high-contrast bursts. Recordings are from the same photoreceptor and LMC.

(**d**) A 600 ms segment of the recordings (from **b**) illustrates how an LMC generates ultrafast, inverted biphasic on/off responses (down- and up-arrows) to the slower, more monotonically rising and falling photoreceptor responses. While the photoreceptor outputs reflect low-frequency changes in light intensity, the LMC transforms this input into high-frequency transients, effectively *transposing* the slow signal into a faster carrier band.

(**e**) Signal-to-noise ratios of the bursty light stimulus and the resulting photoreceptor and LMC responses (from **b** and **d**) demonstrate how synaptic high-frequency jumping causes LMC responses to effectively double the base frequencies of the original light stimulus patterns. This results in LMC responses displaying an effective signalling bandwidth of approximately 920 Hz (signal-to-noise ratio > 1), compared to the photoreceptor responses and the light stimulus at approximately 230 and 600 Hz, respectively.

Together, our results from individual neurons and across populations (**Supplementary Figures 2**, **3**, **5** and **6**; **Supplementary Tables 1**, **2** and **4**) show that housefly photoreceptors and LMCs preferentially encode fast, burst-like changes in light intensity—similar to those encountered during high-speed saccadic movements[9]. These findings highlight a fundamental limitation of neural coding under unnatural steady-state conditions (e.g., prolonged exposure to bright backgrounds with GWN stimulation), which artificially elevate refractoriness, reduce quantal integration efficiency, and suppress neural responses[46,48,49].

Synaptic High-Frequency Jumping Accelerates Vision

Because rapid saccadic flight behaviours are often thought to momentarily "blind" flies through motion blur[33], we investigated how accurately the housefly photoreceptor–LMC superposition system encodes fast-changing visual inputs. **Figure 2d** illustrates, with high temporal resolution, how typical R1–R6 photoreceptors and LMCs respond to a bursty sequence of saccadic light fluctuations. Both photoreceptor and LMC responses were nearly noise-free (**Supplementary Figures 2b** and **5b**), faithfully tracking repeated bursts of contrast. However, their voltage waveforms differed markedly.

Photoreceptors responded to stimulus intensity with relatively smooth, continuous signals. In contrast, LMC responses consisted of sharp, ultrafast transient signals, precisely aligned to the rising and falling phases of the photoreceptor response (**Figure 2d**, yellow box with up/down arrows). These transients were temporally locked to contrast changes and effectively segmented the input signal into a string of biphasic events.

Comparing stimulus and response bandwidths revealed that LMC signals consistently shifted toward significantly higher frequencies, reliably encoding information up to ~920 Hz (signal-to-noise ratio > 1; **Figure 2e**). This *synaptic high-frequency jumping* far exceeded both the reliable stimulus bandwidth (~600 Hz) and the photoreceptor's encoding limit (~230 Hz in this example). Thus, the

biphasic nature of LMC responses (**Figure 2d**, below) effectively doubled the frequency content of their photoreceptor inputs (above), efficiently and instantaneously accentuating transitions in the photoreceptor signal to enhance temporal precision, enabling the synapse to resolve events with ~0.5 ms precision (**Supplementary Video 1**).

Thus, during rapid saccadic visual input, the photoreceptor–LMC circuit employs high-frequency jumping to accelerate vision—shifting neural signals into higher-frequency carrier bands where fast transients can be more effectively represented and transmitted — a strategy that mitigates motion blur and supports high-speed, predictive control of behaviour.

High-Frequency Jumping Maximises Neural Information

We next investigated how high-frequency jumping affects information transfer between R1–R6 photoreceptors (**Figure 3a**) and LMCs (**Figure 3b**) under diverse visual stimuli. To simulate realistic conditions encountered during rapid, cluttered flight, we used ten saccadic light patterns and five randomised light patterns (Gaussian white noise, GWN) as controls (**Figure 2c**).

Photoreceptor responses (**Figure 3a**) showed that faster saccadic stimuli broadened their effective signalling bandwidth (signal-to-noise ratio > 1) to ~440 Hz. Variations across recordings (*cf*. **Figure 2e**) reflected natural differences in the number of microvilli—the photon-sampling units forming the photoreceptor's light-sensitive part, the rhabdomere, whose length and thickness vary across the compound eye (**Supplementary Figures 17-19**). This bandwidth expansion substantially increased their information content (**Figure 3c**, left). Notably, these intracellular recordings typically exceeded the classic flicker-fusion frequency for *Musca* (~230 Hz)[52], which was originally derived from electroretinograms—extracellular field potential measurements that underestimate local neural performance by averaging spatial and temporal signal variations, background activity, and noise across the eyes[18].

LMC responses (**Figure 3b**) exhibited even stronger phasic activity under the same conditions. Synaptic high-frequency jumping redistributed photoreceptor signals into higher-frequency carrier bands, greatly extending LMC bandwidth (**Figure 3c**, right). This effect was most pronounced during high-frequency, high-contrast bursts, where photoreceptor signal-to-noise ratios reached ~2,000 (**Figure 3c**, left). Under these conditions, LMC bandwidth (~920 Hz, right) more than doubled that of the corresponding photoreceptors (~440 Hz, left), whereas GWN stimuli (**Figure 3d**) produced only modest increases (photoreceptors: ~210 Hz, left; LMCs ~255 Hz, right). These results underscore GWN's limitations in evaluating naturalistic neural coding[1,9,46,49], particularly for fast, behaviourally relevant inputs.

With improved high-frequency signal-to-noise ratios, photoreceptor information transfer rates
(**Figure 3e**, left) peaked at ~1,200–2,500 bits/s during 200 Hz saccadic stimulation—compared to
~600–1,000 bits/s under GWN. Corresponding LMC rates (**Figure 3e**, right) were 2–3 times higher,
reaching ~2,500–4,100 bits/s. These are likely the highest neural information rates reported to date
and more than double those previously measured in *Calliphora* photoreceptors and LMCs under
GWN[41]. Thus, the housefly's morphodynamic neural superposition system appears explicitly tuned
to encode fast saccadic inputs with exceptional efficiency and minimal noise—far surpassing
conventional expectations[44,53,54].
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Figure 3. High-frequency jumping maximises information transfer to LMCs during fast, high-contrast saccadic bursts.

(**a**) Analysis of R1-R6 photoreceptor signalling performance was based on intracellular voltage responses to repeated 2-s light patterns across 15 different stimuli.

(**b**) Similar analyses were conducted for LMCs to compare their responses to those of photoreceptors across all the stimuli.

(**c**) **Left**: in R1-R6s, faster saccadic stimulation (right arrow) expands effective signalling bandwidth up to ~440 Hz (indicated by dotted lines, where the signal-to-noise ratio >1), increasing information content. **Right**: in LMCs, high-frequency jumping reallocate this enhanced information across their entire bandwidth (up arrow), elevating the signal-to-noise ratio and achieving effective signalling up to ~920 Hz (excluding the slowest 20 Hz bursts, pink trace).

(**d**) **Left**: Photoreceptors' effective signalling bandwidth massively expands with stimulus contrast. For high-contrast saccadic bursts (c ≈ 1.29), the maximum signal-to-noise ratio reaches ~2,000, and the bandwidth doubles to ~440 Hz, compared to low-contrast Gaussian white noise (GWN; c ≈ 0.33) where the maximum signal-to-noise ratio is ~100 with an effective bandwidth of ~210 Hz. **Right**: LMCs' effective signalling bandwidth also increases and broadens with stimulus contrast. High-frequency jumping is notably more effective during high-contrast bursts than with GWN. As a result, during saccadic stimuli, LMCs' effective signalling range extends to over twice that of photoreceptors, reaching ~920 Hz. Whereas with GWN, the LMCs' effective signalling range is only slightly wider, ~255 Hz, compared to the photoreceptors' ~210 Hz.

(**e**) Photoreceptors' information transfer rates peaked for 200 Hz high-contrast "saccadic" (bursty) stimulation, with the highest estimates reaching about 2,500 bits/s. Their information transfer rates during GWN stimulation were 2-to-3-times lower.

(**f**) LMCs' information transfer rates were 2-to-3-times higher than those of photoreceptors, reaching up to 4,000 bits/s (in one male fly). These estimates typically peaked for 100 Hz or 200 Hz high-contrast "saccadic" bursts. The corresponding information transfer rates during GWN stimulation were 2-to-3 times lower. (**e**, **f**) Thin line, individual cells; thick, mean ± SD. The cell-to-cell variations in information transfer rate estimate likely reflect variable microelectrode recording locations and the eye's sexual dimorphism.

While our intracellular recordings clearly demonstrate the crucial role of synaptic high-frequency

jumping in maximising information transfer during saccadic stimulation—mimicking information flow

during high-speed behaviours—they cannot fully explain the underlying biophysical mechanisms. To

address this, we systematically tested our multiscale model of the morphodynamic neural

superposition system (**Figures 1c** and **4**), directly comparing its predictions with experimental

intracellular recordings and performance analyses.

Figure 4. Morphodynamic neural superposition model: high-frequency jumping and hyperacuity emerge from parallel photoreceptor inputs shaped by multilayered interactions.
(**a**) **Model architecture**. R1–R6 photoreceptors from neighbouring ommatidia sample light through a "flower pattern" of partially overlapping receptive fields (RFs). **Feedback loop 1** (top): Individual microsaccades dynamically shift RFs in response to local contrast changes, driving stochastic quantum bump sequences and adapting the receptive field positions. **Feedback loop 2** (bottom): Voltage differences between R1–R6 photoreceptors trigger quantal histamine release, which binds to postsynaptic chloride channels on LMCs, generating hyperpolarising responses. This engages excitatory synaptic feedback from LMCs to photoreceptors, balancing synaptic loads and enabling fast, phasic signal transmission.
(**b**) **Biophysical signal flow during high-speed stimulation (200 Hz).** Top to bottom: photon absorption in R1–R6 during microsaccades; neural responses; histamine release probabilities and quantal output; resulting LMC voltage; and depolarising synaptic feedback. Simulated responses (blue/red) closely match in vivo recordings (black/grey), demonstrating the model's precision.
(**c**) **Complete model reproduces high-frequency jumping**. Signal-to-noise ratios (SNRs) of both recordings and simulations show high reliability across a broad frequency range under bursty stimulation, confirming the emergence of high-frequency jumping in LMCs. Note: L1/L2 LMC-subtypes receive "identical" histaminergic input from R1–R6[18,55,56], and their On/Off polarities[57] only emerge downstream in the medulla, likely shaped by their distinct neurotransmitters and local circuitry.
(**d**) **Single input disrupts high-frequency jumping**. Driving the LMC with input from only one photoreceptor (here R1) removes high-frequency jumping and reduces SNR.
(**e**) **Slower transmitter release suppresses high-frequency jumping**. Reducing synaptic speed lowers temporal resolution and disrupts high-frequency structure in LMC output.
(**f**) **Phase locking persists without microsaccades**. A static-eye model (no photomechanical input) still supports high-frequency jumping due to intrinsic morphodynamic sampling.
(**g**) **Information rates match recordings**. Simulated R1-R6 and LMC responses across stimulus bandwidths carry similar information to real recordings, peaking near 200 Hz. Mean and SD of the recordings in **Figures 3e** and **3f** (thin grey trace, R1-R6 recording with the highest rates).
(**h**) **Model resolves hyperacute visual features**. Incorporating morphodynamic microsaccades, the model reproduces LMC recordings by resolving single and paired moving dots at separations of 0.7°, 2.1°, and 3.5°. In contrast, a static-eye model (red traces) with receptive fields overcompletely tiling visual space (optophysically accurate)[11,34] achieves only limited hyperacuity (~2.1° separation). A traditional fused-RF model[35,36] (purple traces), which assumes identical R1–R6 responses and perfectly overlapping receptive fields, fails entirely to resolve closely spaced dots—the limit being the interommatidial angle ($\Delta\Phi_{mean}$ = 2.9°). See **Supplementary Figures 11–14** for R1–R6 hyperacuity.

Multiscale Interactions Induce High-Frequency Jumping

The morphodynamic photoreceptor-LMC neural superposition model (**Figure 4a–b**) accurately replicates experimental data and elucidates the mechanistic origins of high-frequency jumping (**Figure 4c**; **Supplementary Figures 28–34**). Simulations show that LMCs' transient responses (**Figure 2b**)—and thus high-frequency jumping—arise during the parallel tonic[16-18,58] quantal histamine release from six photoreceptors (R1–R6) into a shared LMC. Importantly, high-frequency jumping is not the result of a single mechanism but emerges from concurrent adaptive interactions between pre- and postsynaptic processes, as illustrated by two major circular feedback loops (**Figure 4a**).

The model reflects the compound eye anatomy: R1–R6 photoreceptors from neighbouring ommatidia have partially overlapping receptive fields, forming a "flower pattern"[11,34] (**Figure 4a**). In

the first feedback loop (top arrow circle), these receptive fields react to a spatiotemporal light stimulus (green disk) with microsaccades—tiny, directionally varied shifts driven by stochastic refractory photon sampling and photomechanical transduction in ~41,000-74,000 microvilli per photoreceptor. This morphodynamic sampling generates diverse quantum bump sequences and voltage responses across R1-R6 (**Figure 4b**, top three traces), dynamically tuning each photoreceptor's receptive field to local stimulus changes.

In the second feedback loop (bottom arrow circle), differences in R1-R6 voltages modulate their tonic histamine release probabilities. Histamine binding to LMC receptors triggers Cl⁻ influx (left) and produces hyperpolarising postsynaptic responses[16,18,19,59]. The LMC thus integrates quantal input from six photoreceptors with partially overlapping receptive fields, boosting visual information flow to the brain[16,18,57,60] while suppressing aliasing[9,11]. Simultaneously, LMC signals provide excitatory feedback to photoreceptors, maintaining their tonic readiness. By continuously balancing excitatory and inhibitory loads[17-19,56,61], this feedback ensures phasic and undelayed synaptic transmission.

To identify the components essential for high-frequency jumping, we systematically disabled or modified key mechanisms within the model. Simulations, consistent with the data processing theorem[48,62], revealed that pooling signals from all six photoreceptors is critical (**Figure 4d**). A single photoreceptor–LMC synapse, even under ideal noise-free conditions, transmits no more information than the photoreceptor itself. Tonic quantal release alone—e.g. in a single R1–LMC connection—introduces background noise, reducing the LMC's signal-to-noise ratio and preventing high-frequency jumping. In contrast, pooling slightly variable conductance changes from six photoreceptors (**Figure 4b**)—each with a signal-to-noise ratio >1,000 (**Figure 3**)—naturally cancels this noise[9]. Pooling increases the collective photoreceptor output six-fold, driving the synapse to progressively "clip" the extremes of these near-noise-free bursts (see **Supplementary Information, Section IV.11**). This clipping produces a square-like waveform, injecting high-frequency (>500 Hz) components that extend the LMC response bandwidth to nearly 1,000 Hz and enable in vivo-like high-frequency jumping (**Figure 4c**). This *clipping effect*, which boosts high-frequency signals *over time*, resembles the *slit effect*, where an occluding object temporarily narrows a photoreceptor's receptive field to yield hyperacute resolution *over space* (see **Supplementary Information, Section II.8**; **Supplementary Figures 20** and **21**).

Another crucial requirement is the speed of quantal transmitter release, particularly in the photoreceptors (**Figure 4e**), though feedback synapses also play a role. Slower release weakens the histamine release probability modulation, making LMC responses more low-pass and photoreceptor-like. This reduces the high-frequency signal-to-noise ratio and impairs high-frequency jumping. Moreover, removing excitatory feedback from lamina interneurons to photoreceptor

terminals substantially degrades both photoreceptor and LMC signal fidelity, consistent with experimental findings (**Figure 4g**)[18,63].

Interestingly, the model suggests that microsaccades contribute only indirectly to high-frequency jumping. Even in simulations with static (non-moving) photoreceptors, high-frequency jumping persists if synaptic feedback is preserved, though with altered dynamics (**Figure 4f**).

Microsaccades introduce variability due to asymmetric, stochastic and slightly asynchronous R1–R6 movements. In a neural superposition system, this results in small timing offsets—where one photoreceptor may activate before another. This temporal variability reduces the estimated information transfer rates of both photoreceptors and LMCs by ~10% (**Figure 4g**). For example, simulated LMCs transmit an average of 3,063 bits/s with static photoreceptors, compared to 2,732 bits/s with microsaccadic sampling.

Still, this modest reduction is a small trade-off. Microsaccadic motion—arising from the asymmetric, rotated rhabdomere arrangements across neighbouring ommatidia—enables ultrafine hyperacute perception[9,11] (*cf*. **Supplementary Figures 11–14** and **20**), enhancing the compound eye's spatial acuity[9,11] from the anatomical limit of ~2.9° to below 0.7°, a more than fourfold improvement (**Figure 4h**).

In summary, the second (synaptic) feedback loop plays the primary role in enabling temporal high-frequency jumping by coordinating phasic LMC responses to pooled inputs (**Supplementary Video 1**). The first (photoreceptor) feedback loop, by contrast, primarily enhances spatial acuity, generating asymmetric "flower pattern" receptive field motion (**Supplementary Video 2**) that sharpens object resolution, especially for moving objects (**Figure 4h**), and combats spatial aliasing[9,11].

Morphodynamics Matching Visual Lifestyles

In houseflies, as in *Drosophila*[9] and honeybees[10], photoreceptors contract photomechanically in response to changes in light intensity. However, in *Musca*, these movements—driven by refractory photon sampling reactions[1,2,9-11,37]—occur much more rapidly, reducing saturation and more effectively maximising phasic information[9] (**Figure 5a–c**). This faster refractory quantal sampling improves the signal-to-noise ratio at higher stimulus frequencies (**Figure 5e**). For example, *Musca* R1-R6 photoreceptors integrate voltage signals three to four times faster than those in *Drosophila*, as reflected in their effective signalling bandwidths: ~308 Hz versus ~72 Hz for the same 20 Hz bursty stimulus.

Consequently, a typical R1-R6 photoreceptor in a fast-flying housefly samples approximately three times more information from the same stimulus than its slow-flying *Drosophila* counterpart, which

has roughly half as many microvilli (~30,000) and exhibits slower refractory and quantum bump dynamics[9,42,43,46,50]. During high-contrast saccadic bursts, *Musca* photoreceptors reach maximal information rates of ~2,510 bits/s (**Figure 3e**), compared to ~850 bits/s in *Drosophila*[9] (**Figure 5d**).

When six neural superposition photoreceptor outputs—each modulated by its own microsaccades—are combined with top-down synaptic feedback, visual information can be frequency-shifted into biphasic and aliasing-free phase-locked LMC responses. These transiently amplify even the smallest changes in environmental light contrast with minimal delay. In both species, this rapid, bidirectional information flow eliminates classical synaptic delay: photoreceptor and LMC responses begin rising simultaneously (*Musca* ~3.5 ms; *Drosophila* ~6.5 ms after stimulus onset) (**Figure 5b**). Yet in both cases, LMC responses peak significantly earlier than their corresponding photoreceptor inputs—by ~4 ms in *Musca* and ~13 ms in *Drosophila*—consistent with predictive coding mechanisms operating at the synapse (**Supplementary Figure 1a, b**). *Musca*'s faster LMC responses (**Figure 5a–c**) match its quicker behavioural reactions and its need to time-lock visual processing to fast motor outputs.

These findings suggest that evolution has tuned visual information processing to meet each species' behavioural demands—adjusting microvillus numbers, refractory periods, quantum bump dynamics, photomechanical responses, membrane conductances, and synaptic connectivity—while also constraining metabolic cost[9,46,47] (see **Supplementary Information, Section IV**). As a result, housefly photoreceptors and LMCs jointly encode contrast changes at roughly twice the speed of those in *Drosophila*[9] (**Figure 5a–c**).

Figure 5. Morphodynamic sampling and synaptic transmission are adapted to species-specific visual behaviours.

(**a**) **Anatomical specialisations**. *Musca* photoreceptors contain ~54,000 microvilli—nearly twice as many as *Drosophila* (~30,000)—providing greater capacity for light sampling. The average interommatidial angle is also smaller in *Musca* (2.9° vs. 4.5°), enhancing spatial acuity.

(**b**) **Photomechanical microsaccades**. *Musca* R1–R6 photoreceptors exhibit smaller, faster microsaccades than those in *Drosophila*, enabling higher temporal resolution.

(**c**) **Ultrafast neural transmission**. In both species, LMC responses are biphasic and peak earlier than photoreceptor responses, with no detectable synaptic delay (see also **Supplementary Figure 1**). In *Musca*, R1–R6 responses to a 10-ms flash reach their peak within 10–16 ms, aligning with the onset of visually guided behaviours (*cf*. **Figure 6**).

(**d**) **Temporal structure of saccadic responses**. R1–R6 voltage responses to bursty (20 Hz) saccadic contrast changes show clear, phasic dynamics in both species, but *Musca* responses lead those of *Drosophila* in phase.

(**e**) **Signal-to-noise ratio (SNR)**. *Musca* photoreceptors maintain reliable signalling (SNR > 1) across a broader frequency range than *Drosophila*, supporting high-speed visual processing.

(**f**) **Information transfer**. *Musca* R1–R6 photoreceptors transmit up to three times more information than those in *Drosophila*, peaking at 200 Hz for high-contrast bursts—twice the optimal frequency observed in *Drosophila* (100 Hz). Dotted box highlights the information rates for the data in **d** and **e**.

Predictive Coding Enables Ultrafast Behaviours

Next, we investigated whether ultrafast morphodynamic processing, combined with high–frequency–jumping–induced acceleration of neural signalling, is also reflected in the speed of *Musca*'s visually triggered behaviours (**Figure 6**). To test this, we employed two behavioural paradigms that yielded similar results. First, binocular light flashes elicited rapid antennal movements (**Figures 6a–d**), potentially allowing the fly to gather additional olfactory, auditory, or thermal information to reduce stimulus-related uncertainty. Second, when startled by a rapidly looming dark object, a tethered *Musca* exhibited a synchronised, rapid lift of all six legs (**Figures 6e–h**; **Supplementary Video 3**).

Strikingly, the shortest response latencies ranged from 13 to 16.8 ms. These exceptionally brief delays are remarkable because the behaviours appear voluntary and decision-based—conditions typically associated with greater response variability and a higher likelihood of no response[1,64]. In both cases, neural signals must first be generated in the photoreceptors and then transmitted through brain circuits (e.g. **Supplementary Video 4**). Even the most direct "reflex-like" pathway—bypassing central decision-making—would involve at least five synapses (see **Supplementary Information, Section VI**) before reaching the muscles. Yet both responses were highly variable in timing and often absent, distinguishing them from classic, involuntary reflexes[65].

To estimate the minimal possible reaction time, we extrapolated from the complete *Drosophila* brain connectome, adjusting for *Musca*'s brain being approximately three times larger (see **Supplementary Information, Section VI**). Using standard values for synaptic transmission, neural charging, and conduction delays within a unidirectional signalling model (**Figures 6h–i**; see Methods), we predicted a minimum reaction time of 18–29 ms for reflex-like pathways, containing four to six synapses. These predicted delays are 5–16 ms (38%-123%) longer than the shortest observed voluntary response latencies.

Figure 6. Voluntary behavioural responses in flies outpace classical conduction-delay predictions, even along the shortest neural pathways—revealing accelerated sensorimotor processing.
(**a**) High-speed infrared videography (1 kHz) was used to track *Musca* antennae responses to a brief UV light flash. Antennal motion was recorded relative to stimulus onset to measure reaction times.

(**b**) Cross-correlation of antennal motion traces revealed that the shortest reaction latencies occurred within 13-18 ms (left), while more typical responses peaked around 24-25 ms (right), indicating variability across trials.

(**c**) The broad distribution of reaction times suggests that antennal responses are not reflexive but instead voluntarily modulated. Some flies responded consistently, others sporadically, and some not at all.

(**d**) A candidate antennal response circuit comprising 5 synapses was reconstructed using the *Drosophila* connectome and scaled to *Musca* using X-ray microtomography. Standard estimates predict a minimal unidirectional pathway latency of ~21-29 ms. This is 8-16 ms (up to two times) slower than the fastest observed 13 ms antennal responses, implying the involvement of in vivo acceleration mechanisms (e.g., synaptic high-frequency jumping).

(**e**) In a separate setup, tethered flies were presented with high-speed looming stimuli via a 360 Hz projector and back-projection screen, while leg-lift responses were recorded using a 2.5 kHz high-speed camera.

(**f**) Reaction times to looming stimuli varied substantially across individuals and trials. The fastest responses were detected after 16.8-18 ms, with others occurring at 32, 42, or even >100 ms post-stimulus, suggesting a mixture of voluntary and non-responses.

(**g**) Distribution of leg reaction times reveals a multimodal pattern, again consistent with voluntary rather than reflexive control.

(**h**) The leg-lift pathway includes at least 4 synapses and spans ~1.1 mm in conduction length to giant fibres (GFs). Using standard assumptions (Methods), the fastest expected motor response would take ~18-22 ms. Yet observed leg responses at 16.8 ms are 1.2-5.2 ms faster than predicted, reinforcing the idea that classical serial conduction models underestimate the true speed of visual processing in active fly behaviour.

This discrepancy suggests that *Musca*'s neural processing is not strictly feedforward. Instead, it likely involves continuous bottom-up and top-down interactions across brain circuits[17,18,64]. Within this predictive framework, the fly's internal state—its ongoing intentions and behavioural context—modulate sensory processing[1,66-68] and synchronise perception across the brain. We propose that this global feedforward–feedback interplay uses high-frequency jumping to bind object features across space and time, enabling predictive, phasic information flow powered by quantal, refractory, and morphodynamic mechanisms—mirroring those observed at the photoreceptor–LMC synapse (**Figure 4**).

Discussion

Integrating multiscale experimental and modelling approaches, we uncover *synaptic high-frequency jumping* and explain how it emerges. This previously undescribed mechanism enables peripheral visual neurons to shift information into higher carrier frequencies in response to high-speed saccadic input, thereby minimising communication delays and increasing the coding speed of reliable vision. Remarkably, housefly LMCs can transmit information at rates exceeding 4,000 bits/s and operate at bandwidths approaching 1 kHz—far beyond classical flicker-fusion limits[52]. Using ultrahigh-speed videography, we further show that houseflies initiate voluntary, stimulus-triggered behaviours at a time when photoreceptor responses are only just reaching their peak.

These findings challenge long-standing models of sequential neural transmission and reveal how vision dynamically adapts to behavioural demands. Rather than passively processing visual information, houseflies actively shape their sensory input through high-speed flight behaviours,

generating the spatiotemporal structures that drive high-frequency jumping, predictive coding, hyperacute perception and rapid neural synchronisation with environmental dynamics.

By highlighting the critical roles of saccadic visual behaviours, morphodynamic mechanisms, and bidirectional synaptic interactions in enabling fast, parallel, low-latency information sampling and processing, our results have broad implications for understanding efficient encoding and predictive coding. In particular, synaptic high-frequency jumping provides a neurophysiological solution to the binding problem—that is, how information encoded across distinct brain circuits is synchronised to produce unified perception, decision, and action—within the physical constraints of neural computation.

High-Speed Saccadic Behaviours Enhance Vision

Houseflies maintain superior visual performance during rapid saccadic turns generated by flight manoeuvres. These self-induced movements do not impair vision; rather, they enhance it. Morphodynamic neural superposition enables photoreceptors and downstream circuits to extract temporally structured, behaviourally relevant features with minimal delay, enabling simultaneous efficient processing of high-speed visual information and hyperacute perception. The resulting phasic signals are rapidly amplified and undergo synaptic high-frequency jumping, emerging as transient, biphasic LMC responses that broaden bandwidth and shorten latency. These signals are further accelerated by the brain's bidirectional information flow, where tonic feedforward (inhibitory) and feedback (excitatory) interactions help balance synaptic load[1,17-19,61]. As a result, they become synchronised with internal motor states, generating a predictive, time-locked encoding of environmental dynamics—facilitating high-speed decision-making and stable visual perception, even under variable lighting conditions.

Information throughput increases with the number of samples, assuming constant conditions[1,47,48,62]. Photoreceptors continuously adapt to fluctuating light intensities—reflecting logarithmic changes in environmental photon rates—through *refractory quantal sampling*, which dynamically adjusts the quantum efficiency of microvilli[1,9,46,50]. This mechanism enables signal-to-noise ratios of ~1,000–8,000 (e.g. **Figure 5e**) in response to fast saccadic contrast changes under bright daylight conditions. Approximately 54,000 microvilli per cell engage in stochastic sampling, effectively absorbing $~10^5$–10^6 photons per second. In bright illumination ($>10^7$ photons/s), microvillar refractoriness prevents most absorbed photons from eliciting a quantal response[1,9,46,47,50]. Under these conditions, photoreceptor microsaccades—together with the fly's saccadic flight behaviours—selectively enhance the sampling of contrast changes[1,9,11]. As a result, photoreceptors produce accurate anti-aliased estimates of the dynamic visual scene without saturating their biophysically limited amplitude or frequency ranges, while averaging out residual noise[1,9,46,50]. Their histaminergic synapses can thus respond reliably and efficiently to even the slightest contrast changes.

Each LMC integrates slightly variable inputs from six photoreceptors, or seven in the male's frontal-dorsal "love spot" region[52], via overlapping, photomechanically moving receptive fields. This morphodynamic pooling of parallel photoreceptor outputs enhances spatiotemporal resolution, enabling hyperacute pattern detection and object tracking well below the ~2.9° limit imposed by the average interommatidial angle (**Figure 4h**), which defines the static pixel resolution of the compound eye. Remarkably, our recordings and simulations show that the morphodynamic neural superposition system, evident in LMC voltage responses, can resolve moving objects separated by just 0.7°—narrower than the ommatidial lens's airy-disk angle (1.1°), the theoretical diffraction limit (**Supplementary Information, Section II.8**, **S-Figure 20**)—a performance once thought impossible[33].

Notably, high-frequency jumping is absent in recordings using Gaussian white noise (GWN; **Figure 3d**), which increases refractoriness and desensitises phototransduction[9,46]. It is also missing from responses to linearly presented naturalistic image time series, dominated by slow frequencies ($1/f$ statistics)[9,18,48,69]. Our results therefore suggest that animals' *active vision*—combining high-speed saccadic movements with brief fixation pauses[9], including photoreceptor microsaccades[11,12,27], intraocular muscle contractions[70], and eye, head, and body rotations[38]—actively drives high-frequency jumping. This, in turn, enhances the phase congruency of visual features (such as edges, occluding objects, changing textures, and outlines), making them stand out instantaneously in the scene.

Behaviour-Dependent Neural Synchrony

During wakefulness, and especially during active behaviour, flies exhibit heightened visual responsiveness[64,67,71]. Photoreceptor–LMC synapses operate tonically, maintaining continuous interactions between bottom-up sensory input and top-down modulation to support attentional readiness[16-18,58,72]. This dynamic state allows the generation of widespread time-locked neural responses in reaction to behaviourally relevant environmental stimuli.

To understand how high-frequency jumping supports predictive sensorimotor processing, we examined the timing of photoreceptor and LMC responses to rapid stimuli. For example, *Musca* LMCs generate maximum responses within 6.5-9 ms of light onset (mean: 7.6 ± 0.8 ms, n = 10)—well before the associated photoreceptor voltage reaches its peak 5-9.5 ms later (p = 0.012), at 9-16 ms (mean: 11.6 ±1.9 ms, n = 20, **Supplementary Figure 1a**). Similarly, the fastest reaction times during voluntary vision-driven behaviours fall within 13-20 ms (**Figure 6**; **Supplementary Figure 1c**), far shorter than expected under conventional unidirectional transmission models. These findings suggest that high-frequency jumping supports both local synaptic efficiency and global network synchronisation, enabling ultrafast, predictive sensorimotor responses.

To assess whether these principles generalise beyond the first visual synapse, we reexamined response timings deeper in the fly brain. Supporting high-frequency jumping and morphodynamic synchronisation as general neural strategies, minimal-delay responses were also observed downstream in the *Drosophila* visual system[1,64]. In tethered flying flies, electrical activity recorded from the lobula and lobula plate (**Supplementary Figure 1d**)—at least three synapses downstream of photoreceptors—appeared within ~15-20 ms of stimulus onset[64], closely time-locked to *Drosophila* LMC transients (**Figure 5C**; **Supplementary Figure 1b**). Likewise, an 18 ± 1.5 ms (mean ± SD) delay was recorded in the firing of *Drosophila* giant fibres—a pair of large command interneurons, four synapses downstream of photoreceptors, involved in collision-avoidance reactions—in response to light-off stimuli[73,74]. This ultrafast signal propagation, in which transient light changes evoke near-synchronous, minimal-delay activity across the optic lobes in different experiments, further challenges classical models that assume strictly sequential processing with substantial phototransduction, synaptic, and conduction delays.

Thus, information processing in vivo appears more synchronised and integrated, with signals coordinated across multiple brain regions. This is reflected in the fly brain's broadly distributed and dynamic energy use during activity[75]. Rather than conveying information sequentially like falling dominoes, neurons are coupled through morphodynamic and bidirectional synaptic interactions—with high-frequency jumping providing interlinked "strings" that cause the dominoes to fall together. Such synchronised, minimal-delay processing—from sensing to decision-making—is likely essential for supporting complex behaviours in real time.

Implications for Neural Systems

Analogous to recent concepts of human eye movements[76-78], synaptic high-frequency jumping dynamically shifts neural processing of saccadic inputs into higher-frequency domains, enhancing predictive power and visual acuity. Our findings support this broader framework of encoding space through time[9,11,47,76-80]. Specifically, intracellular recordings and biophysically realistic modelling demonstrate how neural circuits actively transform transient visual signals—such as those elicited by saccades—to synchronise perception precisely with high-speed behaviours. This highlights a conserved principle of dynamic, spatiotemporal encoding across diverse visual systems.

Recent studies suggest that synaptic transmission involves ultrastructural mechanical movements[1,5-8,14,15]. Building on this, we propose that high-frequency jumping may be sensitised by stochastic ultrastructural oscillations—morphodynamic jitter—driven by tonic transmitter release. This process may help maintain neural processing and perception in an attentive, ready state at synapses transmitting both bottom-up and top-down signals[1]. Morphodynamic jitter, a form of mechanical stochastic resonance[81,82], could enable interconnected circuits to respond in phase (i.e.,

synchronise) to dynamic or behaviourally relevant inputs, selectively amplifying salient signals while suppressing irrelevant ones. Additionally, jitter could temporally align bottom-up sensory signals with top-down motor predictions[83-85], facilitating faster error correction and behavioural adaptation.

This study underscores the value of an integrative, multi-scale approach to understanding neural systems. By linking molecular, cellular, and systems-level dynamics with high-speed saccadic behaviour, we demonstrate how form, function, and behaviour co-adapt to support robust, adaptive vision in rapidly changing environments—enabling advanced computations already at the level of information sampling. This framework reveals emergent properties—such as high-frequency jumping, efficient coding, hyperacute vision, fast adaptive gain control, and predictive time-locking—that remain obscured when neural components are studied in isolation. For instance, morphodynamic sampling (encompassing photomechanical, stochastic, refractory, and quantal processes) and high-frequency jumping cannot be reproduced by conventional high-level reductionist models that treat photoreceptors and LMCs as static, unidirectional filters.

Beyond insect vision, our findings point to fundamental principles of neural computation. They offer new insights into enduring challenges, such as the neural binding problem, by showing how distributed, time-sensitive signals can be synchronised to generate unified percepts and high-speed, purposeful behaviour. More broadly, these principles could inform the design of next-generation artificial systems that, like biological vision, must operate efficiently under real-time constraints in noisy and dynamic environments.

Looking ahead, uncovering how morphodynamic high-frequency jumping generalises across sensory modalities and species may reveal fundamental laws of biological intelligence—laws that could drive the next revolution in adaptive, real-time artificial systems, from autonomous robots to predictive neuromorphic architectures.

Methods

We provide here a brief overview of the main methods; full details of the multiscale experimental and theoretical approaches are in the **Supplementary Information** (**Sections I–VI**). **Section I** covers analyses of intracellular voltage responses from R1–R6 photoreceptors and LMCs under extended experimental paradigms. **Section II** describes high-resolution X-ray and electron microscopy (EM) analyses of *Musca* compound eye optics and photomechanical microsaccadic sampling underlying hyperacuity. **Section III** explains in vivo high-speed optical imaging of photoreceptor microsaccades. **Section IV** details the mathematical modelling of the morphodynamic neural superposition system, incorporating adaptive optics. Finally, **Section V** presents the behavioural experiments, and **Section VI** the functional connectomics of *Musca*.

Fly stocks

Adult wild-type houseflies (*Musca domestica*) were used in the experiments. Housefly larvae and pupae were sourced from a commercial supplier (Blades Biological Ltd, Cowden, Kent, UK). They were cultured in a standard laboratory incubator (60% humidity) at the School of Biosciences and fed liver and sugar water. Flies were maintained at ~22 °C under a 12:12 h light:dark cycle. In some experiments, adult wild-type *Drosophila* (Canton-S) reared separately at 25 °C served as controls[9].

In vivo intracellular recordings

Fly preparation and intracellular recordings were performed as described previously[9,86]. Briefly, houseflies were anaesthetised on ice. Once immobilised, their wings and legs were removed, and they were fixed to a conical holder (brass/plastic) using beeswax, securing the thorax, proboscis, and right eye to minimise movement artefacts. A small hole (covering 6–10 ommatidia) was cut in the dorsal cornea of the left eye to allow electrode access, and sealed with Vaseline to prevent drying[86].

Voltage responses of R1–R6 photoreceptors and L1–L3 lamina monopolar cells (LMCs) were recorded using sharp, filamented borosilicate microelectrodes (Sutter Instruments; 1.0 mm outer diameter, 0.5 mm inner diameter), with resistances of 100–250 MΩ, pulled with a P-2000 horizontal laser micropipette puller. The tip of the reference electrode was cracked to reduce its resistance.

Photoreceptors and LMCs were recorded in separate sessions. Electrodes were back-filled with 3 M KCl for photoreceptors, and 3 M potassium acetate with 0.5 mM KCl for LMCs to maintain the chloride battery. The reference electrodes (blunt-tipped) were filled with fly Ringer solution (120 mM NaCl, 5 mM KCl, 5 mM TES, 1.5 mM $CaCl_2$, 4 mM $MgCl_2$, and 30 mM sucrose)[42]. Under a Nikon SMZ645 stereomicroscope, a remote-controlled micromanipulator (PM10, Mertzhauser) was used to position the electrodes. Thanks to the system's stability, a single recording electrode often penetrated multiple photoreceptors—or occasionally LMCs—in sequence, yielding high-quality recordings from many cells within the same eye.

The fly's temperature was maintained at 25 ± 1 °C using a feedback-controlled Peltier device[42,86]. Only stable, high-quality recordings were analysed. In darkness, R1–R6 resting potentials were < − 60 mV, with responses ≥ 45 mV to 100 ms saturating light pulses. L1–L3 cells showed dark resting potentials < −30 mV and maximum responses ≥ 20 mV. As LMCs were blindly penetrated and not stained, individual cell identities could not be confirmed; however, most were likely L1 or L2 due to their larger size[16-18]. Data from all recorded LMCs were pooled, given their similar response properties, including dark resting potential, hyperpolarisation to light increments, and response amplitudes.

Ruling out efference copy interference in intracellular recordings

Stable intracellular recordings require firmly head-fixed flies to eliminate movement artefacts caused by bodily functions and to minimise recording noise. As a result, the fly cannot perform overt visual behaviours, such as head or body saccades, during stimulation. The saccadic bursty stimuli used in this study, therefore, only mimicked the light intensity time-series patterns (see *Visual stimuli* below) that such behaviours would normally generate. However, the fly could still produce internal motor-related signals—*efference copies*—typically associated with these behaviours[68,83-85].

In our recording paradigm, the fly has no control over the stimulus. Thus, any efference copies generated by its motor circuits and transmitted downstream to photoreceptors or LMCs would not be synchronised with, or predictive of, the stimulus-driven responses. Instead, any such top-down signals would appear as sporadic, uncorrelated noise in the recordings.

Over the past 30 years, we have refined our bespoke intracellular recording systems to achieve exceptionally low noise levels[9,16,42,43,47,63,86]. This enables us to accurately quantify neural responses and distinguish signal from noise under various visual conditions. Our signal-to-noise analyses of photoreceptor and LMC responses (see *Data analysis* below) have never revealed extrinsic noise patterns consistent with efference copies.

Indeed, all observed photoreceptor noise (variability in processing) can be fully explained and reconstructed from four well-characterised sources (see **Supplementary Information, Section IV**):

- *Quantum bump noise*[42,43], modelled as a Lorentzian derived from the Gamma-shaped bump profile
- *Microsaccade noise*[9], introducing a low-frequency hump
- *Synaptic feedback noise*[18] from LMCs and amacrine cells, adding high-frequency Poisson-like variability shaped by the LMC waveform
- *1/f instrumental recording noise*[42,43]

Given this comprehensive account of known noise sources, the likelihood that efference copies influenced our recorded data under this specific experimental paradigm is exceptionally small. Moreover, our morphodynamic neural superposition model—lacking any built-in top-down circuitry—replicates both photoreceptor and LMC response dynamics (e.g. **Figure 4**). Therefore, the present study does not provide evidence for efference copy influence on neural signalling at this early sensory sampling stage.

Visual stimuli

A high-intensity "white" LED (Seoul Z-Power P4 Star, 100 lumens) was used to deliver light stimuli centred on the receptive field via a randomised quartz fibre-optic bundle (180–1,200 nm transmission range) mounted on a rotatable Cardan-arm, subtending a 3° homogeneous light field[86]. Output was controlled by an OptoLED driver (Cairn Research Ltd, UK).

To characterise temporal encoding, five 2-second Gaussian white noise (GWN) stimuli of varying bandwidths (20, 50, 100, 200, and 500 Hz) were presented. These stimuli were generated using MATLAB's randn function, low-pass filtered (MATLAB Filter Toolbox), and scaled to have flat power spectra and equal peak-to-peak modulation (two units). Each bandwidth was tested under three contrast conditions on a linear intensity scale: high (BG0, 0 background light units), mid (BG0.5, 0.5 units), and low (BG1, 1 unit). Contrast was defined using Weber's law:

$$c = \frac{\Delta I}{I} \tag{1}$$

where ΔI is the intensity change (standard deviation of the stimulus), and I is the mean background intensity. Measured contrasts were:

- High-contrast "saccadic" bursts: $c(BG0)$ = 1.29 ± 0.13
- Mid-contrast bursts: $c(BG0.5)$ = 0.61 ± 0.10
- Low-contrast GWN: $c(BG1)$ = 0.33 ± 0.05

Stimuli were presented from the lowest to the highest adapting background. Prior to each stimulus, cells were dark-adapted for 20–30 seconds. Only cells with stable recordings across all 15 stimulus patterns were analysed. However, since LMC recordings are more difficult to maintain than photoreceptor recordings, in some cases only the five bursty stimuli were used for LMCs. Each stimulus was repeated at least 30 times per cell.

Stimuli and responses were low-pass filtered at 500 Hz or 1 kHz (KEMO VBF/23 elliptic filter, UK) and digitised at 1 or 2 kHz using a 12-bit A/D converter (National Instruments, USA). Data acquisition and stimulus control were handled via custom-written software (Biosyst, M. Juusola, 1997–2020) in MATLAB (MathWorks, USA)[42,48], interfaced via the MATDAQ package (H.P.C. Robinson, 1997–2005) for National Instruments boards.

Data analysis

To ensure all the studied cells had reached a similar adaptation state, the first five responses (10 seconds of data) to the repeated stimulus were excluded from both signal and noise analyses. This left at least 25 responses to the same repeated stimulus pattern. The signal was defined as the mean

response, and the noise as the deviation of individual traces from this mean[42,48]. Thus, n repetitions (n = 30) yielded one signal and 25 noise traces.

The signal $s(t)$ and noise $n(t)$ traces were segmented into 50%-overlapping stretches and windowed with a Blackman-Harris 4-term window. Each window produced six 500-point- or 1,000-point-long samples, corresponding to 1 or 2 kHz sampling, respectively. Fast Fourier transforms (FFTs) were applied to compute the frequency-domain signal and noise spectra, $S(f)$ and $N(f)$, respectively. The signal-to-noise ratio in the domain $SNR(f)$ was calculated as:

$$SNR(f) \; = \; \frac{|\langle S(f)\rangle|^2}{|\langle N(f)\rangle|^2} \tag{2}$$

where $|\langle S(f)\rangle|^2$ and $|\langle N(f)\rangle|^2$ are the power spectra of signal and noise, respectively. Here v denotes voltage, $||$ the absolute value, and $\langle\rangle$ the average over all signal and noise windows[42,48].

Information transfer rate (R) was calculated from the $SNR(f)$ using Shannon's information formula[62], which is widely applied in this context[9,46,48]:

$$R = \int_{f_{low}}^{f_{high}} log_2(SNR(f) + 1)df \tag{3}$$

Signals were sampled at either 1 or 2 kHz and windowed accordingly (1,000- or 2,000-point Blackman-Harris window). Therefore, the integration bounds were 2–500 Hz (for 1 kHz sampling) or 1–1,000 Hz (for 2 kHz sampling), not 0 to ∞.

However, for LMC recordings sampled at the lower rate (1 kHz), Eq. 3 underestimates the true information transfer rates—particularly for mid- and high-contrast "saccadic" burst responses— because these evoked high-frequency jumping, with $SNR(f) \gg 1$ at 500 Hz (*cf*. **Figure 2e**), indicating that frequencies above 500 Hz contributed non-negligible information. In contrast, this underestimation was not observed for responses to low-contrast Gaussian white noise (GWN) stimuli, which did not evoke high-frequency jumping and exhibited substantially lower response bandwidths (**Supplementary Figure 7e**).

To correct for the high-frequency jumping effect, information losses in the 1 kHz recordings were estimated by comparison with matched 2 kHz recordings using the same stimuli. For photoreceptors (n = 2), the mean information loss was approximately 5% and consistent across cells. For LMCs (n = 2), the loss ranged from 5–23%, with the largest deficits observed for stimuli peaking near 200 Hz. The information transfer rate estimates for both photoreceptors and LMCs were corrected

using stimulus-specific factors, calculated as the percentage difference between $R_{2-500Hz}$ and $R_{2-1,000Hz}$ as defined by Eq. 3.

Moreover, information transfer rate estimates for LMCs during high-contrast bursts were less reliable than those for photoreceptors because the recorded voltage signals typically deviated from a Gaussian distribution—except when tested with a 500 Hz Gaussian White Noise stimulus (**Supplementary Information**, **Section I**, **Supplementary Figure 4b**). Consequently, Shannon-based information estimates are most accurate under mid- and low-contrast conditions, where voltage responses more closely approximate Gaussian distributions (**Supplementary Figure 7b**). Applying Shannon's method to non-Gaussian responses, which violates its assumptions, may inflate estimates by ~12%, as verified against the assumption-free triple-extrapolation method[48] (**Supplementary Figure 8**).

However, several factors contribute to underestimating the true capacity of the system (**Supplementary Figure 9**). Microelectrode penetrations inherently damage the recorded cells, reducing signal fidelity. Additionally, responses cannot be measured in a true steady state, as they continually reflect ongoing adaptation, network dynamics[17,18,61] and top-down eye-muscle activity[87]. Because recordings are never fully ergodic—trial-to-trial variability arises from adaptive network processes rather than pure noise—standard stationary information analyses mistakenly classify intrinsic or network-driven adaptations as additive noise. Thus, the actual information transfer rates and visual performance of housefly vision likely surpass our conservative estimates.

These analyses demonstrate that estimates derived from 25 repetitions (excluding the first five responses) are conservative rather than inflated; adaptive trends cause underestimation, not overestimation, of synaptic information transfer capacity. Therefore, our reported values represent a robust lower bound on the actual encoding precision of LMCs.

Flies also counteract motion blur during saccadic behaviours via multiple mechanisms: predictive stabilisation of head and body movements[25,26], enhanced processing in acute zones[88], and photomechanical, refractory light information sampling[9,11]. However, in our experiments, *Musca* were fixed in conical holders, eliminating head and body movement. We also used female flies and did not intentionally target the male acute zone, ensuring that neither electrode placement nor sex biased the results. Thus, the enhanced responsiveness of both photoreceptors and LMCs to fast, saccade-like stimuli reflects high-performance sampling and transmission dynamics[9-11], which have evolved to support the fly's high-speed visual behaviours and lifestyle.

Morphodynamic Neural Superposition System

In the fly's neural superposition eye (as viewed statically), six R1–R6 photoreceptors from different ommatidia converge onto shared downstream neurons (LMCs and an amacrine cell)[89]. Each photoreceptor is optically aligned to sample light from approximately the same region of space—but due to slight angular offsets and biological variability, their receptive fields do not perfectly overlap[11,34]. Instead, they sample from a small, fuzzy area, creating an over-complete, spatially jittered representation of the visual scene (**Figure 1b**).

In a living fly, however, this system operates as a spatiotemporally dynamic morphodynamic network[11]. The receptive fields are not fixed; they shift in space and time due to photomechanical microsaccades—tiny, light-driven rhabdomere movements (**Figure 1b-c**). This adds a temporal dimension to the over-complete spatial sampling, allowing receptive fields to sweep across fine spatial details and generate richer, decorrelated input patterns.

The result is a morphodynamic neural superposition system that enhances information encoding by:

- Dynamically refining receptive field alignment,
- Exploiting redundancy for noise suppression and error correction,
- Supporting high-frequency jumping and predictive coding aligned with behaviour.

This system transforms passive optical overlap into an active, synchronised sampling strategy, optimised for high-speed saccadic vision. **Supplementary Information**, **Section IV** details how we modelled the photoreceptor and LMC responses of this sophisticated morphodynamic system.

Extrapolating Musca reaction times.

To estimate the minimal reaction time of *Musca* antennal and leg responses to visual stimuli, we focused on two fast sensorimotor pathways: the light-induced antennal movement and the looming-induced leg escape response (see **Supplementary Information**, **Section VI**, **Supplementary Figures 38–41**). Although no complete connectomic or genetic dataset exists for *Musca*, the neural architecture underlying the visual system is highly conserved between *Drosophila* and *Musca*[90]. We therefore used *Drosophila melanogaster*, for which complete connectomic data is available. Using the FlyBrainLab platform (see **Supplementary Information**, **Section VI** for details), we identified the shortest reflex-like pathways linking the retina to motoneurons controlling antennal and leg responses (**Figure 6d,h**), with minimal synaptic gaps and conduction distances. Examining these pathways in Drosophila allows us to extrapolate *Musca*'s visual-motor response time.

We accumulate processing delays along the two *Drosophila* pathwaysattributed to phototransduction and voltage integration, synaptic transmission delay, conduction speed (see **Supplementary Information**, **Section VI**). While *Musca* has a larger brain, the main contributors to processing delay,

phototransduction and synaptic transmission, are likely conserved, while a small difference in conduction delays may exist and we consider that the *Musca* has 3 times the body size as that of the fruit fly.

Together, these stages yield an estimated reaction time of 22.5-29.5 ms for the light-induced antennal movement and 18.6-22 ms for the looming induced leg escape response. We propose this as a reasonable lower-bound estimate for these visually induced motor responses in *Musca*, based on highly compact reflex-like pathways and conventional fast signalling assumptions. These estimates are at least 5-9 ms slower than our experimental observations of voluntary visual responses in flies (13 ms), suggesting the involvement of in vivo acceleration mechanisms (e.g., synaptic high-frequency jumping).

Statistics. Statistical analyses were carried out in Python, Origin and MATLAB. Maximum information rates and visual acuity between male and female photoreceptors, and the whole population of photoreceptors and LMCs, were compared. The statistical methods are explained in the **Supplementary Information**, **Sections I-VI**.

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