1

Main Manuscript for

Decoupling liquid-liquid phase separation and opalescence from stress-induced aggregation in therapeutic mAb formulations

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This PDF file includes:

Main Text
Figures 1 to 4
44
45   **Abstract**

46
Liquid-liquid phase separation (LLPS) and high opalescence resulting from attractive interactions
in the absence of large-scale self-association are commonly encountered in liquid monoclonal
antibody (mAb) formulations and often associated with aggregation. Here, we evaluated the
formulation dependent self-assembly behavior of a therapeutic mAb (termed mAb1) and provide
a link to physical stability after applied stress. Using a combinatorial microdroplet platform to
delineate the phase space of mAb1, we highlight its unusual solution properties. Specifically,
mAb1 undergoes LLPS in a narrow window of low NaCl concentrations, in a formulation relevant
design space, at room temperature (RT), without crowding agents and more than one pH unit
lower than its isoelectric point. Using time-resolved small-angle X-ray scattering, we measured
the attractive interactions underpinning LLPS to be on the sub second timescale and leading to
the formation of small clusters, which altogether could be rapidly inhibited by L-arginine HCl. The
elevated opalescence of mAb1 solutions extended beyond the LLPS regime, where a highly
similar interaction fingerprint to the LLPS condition was observed but no microscopic association
was detected. This suggests that LLPS and opalescence differ in the distribution of interactions
within their networks, dictating their ability to form long-range assemblies (phase-separated
droplets) or not. Finally, our physical stability assessment highlights that mAb1 LLPS and
molecular assemblies giving rise to high opalescence both resist stirring stress and that the
observed aggregation is uncorrelated with ionic strength at our selected timescale. This
observation challenges an unequivocal relationship between LLPS/opalescence and reduced
physical stability of mAb solutions.

Significance Statement

68
The development of formulations maximizing the stability of therapeutic monoclonal antibodies is
a crucial part of their successful development. However, their proclivity for self-association often
results in increased opalescence, which has been shown to indicate a propensity for liquid-liquid
phase separation (LLPS), involving the de-mixing of solutions into two phases with different
concentrations of solute. Both phenomena are commonly tied to a high propensity for
aggregation. However, given the paucity of experimental studies, evidence for a general
correlation between these solution properties and aggregation remains scant. In this work, we
decouple stress-induced aggregation from LLPS and high opalescence without large-scale self-
association through the fundamental study of these phenomena and solution integrity after
applied stress.
79
80
81   **Introduction**

82
Since the approval in 1986 by the US Food and Drug Administration of the first monoclonal
antibody (mAb) as a novel drug modality to reduce kidney transplant rejection in humans
(Muromonab-CD3/), their commercial success of has been continuously expanding, with 100

unique mAb products approved as of 2021 for the treatment of a variety of medical conditions (1–
4). Key factors for the success of mAbs as therapeutics include the established and versatile
possibilities for antibody discovery and engineering allowing development of fine-tuned binding
affinities for desired targets (1, 5). Moreover, the interaction between the fragment crystallizable
region of mAbs with the neonatal Fc receptor grants them a prolonged plasma half-life, rendering
less frequent administration possible (2). Therapeutic mAbs are usually administered parenterally
by intravenous infusion or subcutaneous (SC) injection. For chronic disease management, the
latter approach is favored, as it improves patient adherence by providing a less intrusive delivery
method and the ease of self-administration at home.(6–9). However, due to their large size and
often limited potency, mAbs are routinely formulated at concentrations exceeding 100 mg/mL, to
deliver an effective dose at the small injection volumes imposed by the SC route (1-1.5 mL) (9,
10). In these crowded regimes, the probability of collisions between mAb molecules increases
and, if these interactions are more favorable than interactions with the surrounding solvent, they
can result in the formation of higher-order protein networks. This process can trigger various
outcomes as curated in (11), such as the formation of reversible oligomers (clusters) that can
lead to macroscopic effects including high solution viscosity (6, 12, 13), high opalescence (term
often used interchangeably with turbidity) (14) and liquid-liquid phase separation (LLPS) (15, 16)
or the formation of larger soluble/insoluble aggregates (17).

Opalescence is commonly observed in mAb solution and is a light scattering phenomenon that
can arise from different phenomena such as net attractive interactions between molecules without
association into higher order species (18), particulate matter or concentration fluctuations in
solution (19, 20). LLPS is an example of the latter and occurs when solutes spontaneously
associate through weak but multiple, synergistic and noncovalent interactions in solution, often
mediated by surface patches of high local charge density of hydrophobicity (20, 21). This process
is associated with an increased opalescent appearance as a result of the solution separating into
two distinct phases: a highly concentrated, dense phase and a less concentrated, "dilute" phase
(21, 22). Factors such as ionic strength modulation through the addition of salts as well as the salt
type and concentration have been reported to influence mAb LLPS (23). Additional factors
include the proximity of the formulation pH to the isoelectric point (pI) of the mAbs (23–27),
incubation at refrigerated temperatures (≈ 4°C) and below (23, 25, 28–32), the presence of
crowding agents (33), nonspecific interactions with ligands (21) and binding to smaller ionic
additives (24, 34). Protein LLPS in aqueous solutions has been studied for decades (22).
However, since a seminal paper from 2009 demonstrating the generation of biomolecular
condensates *in vivo* through phase separation and their importance in orchestrating cellular
processes, reports of protein systems exhibiting LLPS have multiplied (35).

In a drug development context opalescence above a defined threshold is often avoided in mAb
solutions as it is commonly flagged as a precursor for LLPS (7) and, by extension, aggregation:
two detrimental phenomena for the development of reproducible and high-quality therapeutic
products. LLPS is a development concern for two reasons (1) the delicate formation and
dissociation of LLPS based on changes in temperature, excipients, proteins concentration and
incubation time makes it very difficult to develop proper control strategies during a product's shelf-
life and (2) it has been linked to aggregation of some protein systems (7, 28, 35). The large
majority of reported LLPS-related aggregation concerns disordered protein systems (36, 37). This
was recently corroborated by Linsemeier et al. (38), who observed that the surface of hnRNPA1
droplets could serve as nucleation points for fibril formation. Another study by Soumik et.al (39)
revealed that ageing of phase-separated droplets accelerated the aggregation kinetics of α-
synuclein. Interestingly, while droplet interfaces have been demonstrated to spearhead the
aggregation fof several proteins, more recent reports also point toward a shielding role of the
droplet interior, emphasizing the double-edged nature of this phenomenon (40, 41). Concerning
mAbs, Pantuso et al. hypothesized that LLPS-induced partial unfolding of the Anti-CD20 mAb
promoted crystal growth along the droplet surface (42). On the other hand, Bramham et al.
observed that the structural integrity of the COE3 mAb was conserved upon LLPS formation and

no changes in the aggregation profile were detected after storage at refrigerated conditions (4°C)
after 28 days (43). Hence, a direct experimental link between mAb LLPS and aggregation has to
our knowledge not been established under formulation relevant conditions.

In this work, we aim to study the connection between LLPS and opalescence, as well as their
effect on aggregation upon physical stress using a model therapeutic mAb, termed mAb1 here.
Using a combination of droplet microfluidics, light scattering, and imaging techniques, we show
that low NaCl concentrations induce LLPS of mAb1 above 30 mg/ml in a minimal formulation. The
LLPS phase space is flanked by well-mixed states of differing opalescence levels, representing a
case of mAb reentrant-like phase transition behavior. Time-resolved small-angle X-ray scattering
(TR-SAXS) reveal that the interactions leading to LLPS are formed extremely rapidly (sub second
timescale) and can be inhibited by adding L-arginine HCl. We further report that mAb1 LLPS and
opalescence without large-scale self-association, which can be indistinguishable visibly and in
light scattering properties, are both driven by attractive interactions and argue that differences in
their colloidal interaction landscapes result in the observed different microstructures being formed
in each case. Finally, we evaluated whether LLPS/opalescence increased aggregation, by
subjecting selected formulations to contact magnetic stirring. The observed aggregation is
independent of the ionic strength and the presence of LLPS/opalescence. This suggests the
presence of two decoupled self-assembly mechanisms: one NaCl-dependent pathway and a
stress-induced pathway independent of ionic strength. The former is characterized by LLPS at
low salt followed by a reentrant phase transition to a highly opalescent, droplet-free state in
proximity to the phase border, after which interactions become gradually more repulsive as the
ionic strength increases. The second pathway is induced by stirring stress, yielding similar
aggregation profiles irrespective of the starting condition.
161

162 **Results**

163
164
165 **mAb1 opalescence and liquid-liquid phase separation are modulated by ionic strength**
166
We first investigated the phase behavior of mAb1 as a function of ionic strength at RT in a
relevant formulation buffer consisting of 10 mM histidine at pH 6.5. To achieve this, fresh
solutions of mAb1 were prepared at a fixed concentration of 45 mg/mL and the ionic strength was
varied through the addition of NaCl. Inspection of the resulting solutions revealed a non-linear
relationship between the NaCl concentration and resulting opalescence/turbidity (Figure 1A). With
increasing ionic strength, a high initial degree of opalescence was rapidly observed in the
titration, followed by a subsequent decrease at higher salt concentrations. These observations
were confirmed by the measurement of the light scattering intensity of the samples at a fixed
angle (90°) (Figure 1B). To determine the origin of this high opalescence (which we will refer to as
opalescence from now on), we next investigated selected mAb solutions by brightfield
microscopy: the two extreme conditions of the NaCl titration series (0 and 150 mM NaCl, blue and
green in Figure 1B) and two conditions yielding comparably high scattering intensities (10 and
22.5 mM NaCl, pink and purple in Figure 1B). As shown in Figure 1C, microscopy images of the 0
mM sample showed no clear indications of mesoscale self-association, whereas at 10 mM NaCl,
highly dynamic droplets could easily be visualized, which readily coalesced upon contact and
'wetted' the glass surface of the microscopy slide within seconds, emphasizing their liquid-like
nature (Figure S1). However, at 22.5 mM NaCl, no droplets or other assemblies resolvable by this
technique were detected, in line with the early observation that conditions without any apparent
large-scale association also give rise to a high degree of opalescence (18). Finally, increasing the
NaCl concentration to 150 mM yielded a clear sample, similar to the 0 mM NaCl condition.

187
The presence of both opalescence as a single phenomenon or associated with LLPS in a narrow
NaCl range complicates the determination of the LLPS regime by traditional techniques (e.g.

measurements of turbidity by light scattering). We therefore mapped the phase space over a
broad range of mAb1 concentrations as a function of low NaCl concentrations where we
observed the largest effect, using a high-throughput combinatorial microfluidic-based technique
termed PhaseScan (45). Briefly, this method relies on the precise encapsulation of predefined
combinations of mAb1, buffer (10 mM histidine pH 6.5) and NaCl solutions into
microenvironments surrounded by an oil phase, for which the presence of droplets is individually
assessed via fluorescence detection. As depicted in Figure 1D (and Figure S2), below 5 mM
NaCl, no LLPS was detected at any mAb1 concentrations. By adding as little as 5 mM NaCl,
LLPS was induced at mAb1 concentrations above an approximate apparent saturation
concentration of 30 mg/mL. Remarkably, above 10 mM NaCl, the system returned to its original
state i.e. underwent reentrant phase transition (46–50). Moreover, for most instances of detected
LLPS, a large fraction of the droplets volume consisted of amorphous dense phase with high
translational dynamics, readily adopting new shapes (Figure S3). From these results we can
conclude that, under formulation relevant conditions, mAb1 depicts a complex phase behavior,
displaying reentrant phase transition in a narrow NaCl range. Meanwhile, on the border of the
LLPS spinodal line, opalescence is observed, yielding high light scattering intensities, not caused
by the presence of well-defined dense droplets.

207
LLPS is driven by attractive interactions on the sub second timescale which are inhibited
by L-arginine HCl

Based on the observations above, we further studied the protein-protein interactions underpinning
mAb1 LLPS and opalescence by measuring small-angle X-ray scattering (SAXS) on our selected
formulations at 45 mg/mL (Figure 2A). At high concentrations, the distances between mAb
molecules and intramolecular distances reach similar orders of magnitude as a result of their
dense packing, leading to a measurable distortion of the scattering signal I($\mathbf{q}$) of the mAb alone.
This interparticle contribution, termed structure factor S($\mathbf{q}$), is primarily visible at small scattering
angles (i.e. low $\mathbf{q}$) in the absence of structural reorganization and reports on the presence of
attractive (S($\mathbf{q}$)>1) or repulsive (S($\mathbf{q}$)<1) interactions, which we are interested in here. The
structure factor contribution was obtained by dividing the total scattering intensity by that of a
dilute mAb1 sample devoid of interparticle interactions (form factor) using on-line SEC-SAXS
(Figure S4). By fitting the Guinier region (51) of the obtained form factor, we determined the
radius of gyration of mAb1 to be 50 Å, as expected for a standard monoclonal antibody (Figure
S4D) (52). As shown in Figure 2A, the structure factors for the LLPS (10 mM NaCl) and
opalescent (22.5 mM NaCl) conditions had a similar shape, displaying highly attractive
interactions, as inferred from the linear increase of structure factor at low $\mathbf{q}$. Interestingly,
positional correlation peaks were observed at $\mathbf{q}$=0.06 Å^{-1} and 0.1-0.12 Å^{-1},corresponding to real
space distances of 104 and 52 Å respectively, roughly equal to the diameter and radius of mAb1.
This is in line with the S($\mathbf{q}$) data reported for other mAbs and points toward the formation of small
equilibrium clusters in solution (6, 13, 53, 54). Altogether, this suggests that both LLPS and
opalescence have the same underlying molecular grammar, and that these phenomena therefore
can be mitigated using a similar approach. A common strategy to minimize LLPS/opalescence in
mAb formulations relies on the addition of L-arginine HCl (10, 55). Indeed, adding 150 mM L-
arginine HCl to a formulation in which mAb1 would have otherwise undergone LLPS (10 mM
histidine pH 6.5 + 10 mM NaCl) no LLPS was observed, suggesting an inhibitory effect of L-
arginine HCl on mAb1 LLPS (Figure S5). We further studied the extent of the inhibition of
attractive interactions by L-arginine HCl and compared it to increasing the NaCl concentration to
150 mM, which similarly decreased the scattering and visual opalescence considerably (Figure
1). As shown in Figure 2A, a drastic reduction in the S($\mathbf{q}$) was observed for both conditions, albeit
to a lower extent for the 150 mM NaCl condition, for which attractive interactions could still be
observed compared to the sample containing L-arginine HCl, in which their formation is
completely inhibited. Interestingly, the positional correlations mentioned above were also visible

for these two conditions but with decreased peak definition, probably due to the stronger
screening of electrostatic interactions at higher ionic strengths (56).

Complementary insights into the in-situ phase separation of mAb1 were obtained through time-
resolved SAXS measurements (TR-SAXS), by coupling a microfluidic device to the experimental
setup at the beamline. In this sample environment, the laminar flow in the channels
hydrodynamically focuses their constituent components, which passively diffuse to a junction
point where they are mixed. The temporal resolution is then achieved by measuring SAXS at
different distances from the mixing point on the chip, i.e. depending on the flowrate, each point on
the z axis relates to a specific timepoint after mixing (Figure 2B). This approach enables the
investigation of initial stages of LLPS, offering insights into the characteristics and progression of
protein-protein interactions associated with this phenomenon over millisecond to second
timescales. TR-SAXS experiments were performed by mixing mAb1 in 10 mM histidine pH 6.5
buffer with the same buffer supplied with NaCl to reach the final desired concentrations. Under
LLPS inducing conditions, mAb1 interactions are already highly attractive 12 ms from the mixing
point and remain so throughout the studied time range, demonstrating the rapid nature of the
interactions conducive to LLPS (Figure 2C). This is also highlighted in Figure 2F where the
average of the first three S(q) values at each timepoint of the individual conditions are
summarized for a clearer overview of their temporal evolution. At 10 mM NaCl, the magnitude of
the structure factor increases rapidly before fluctuating around a high mean value. When
inhibiting the formation of dense phase by adding 150 mM L-arginine HCl, the S(q) measured at
the first timepoint of 12 ms was considerably lower compared to the LLPS sample, switching from
attractive to slightly repulsive interactions at 2.4 s (Figure 2D). For the 150 mM NaCl condition, a
relatively higher structure factor was observed at the last timepoint in the TR-SAXS experiment,
suggesting a more efficient suppression of attractive interactions by L-arginine HCl compared to
NaCl, considering the slower diffusion in the mixing channel of the former. In all cases, the
scattering curves of the final timepoints in the time-resolved experiment overlapped with the static
SAXS data, showing a high level of agreement between the two setups (Figure S6).

LLPS/opalescence and stress-induced aggregation of mAb1 are decoupled

As a final step in the present study, we subjected our mAb1 formulations to overnight vigorous
stirring (18 hours at 1000 rpm, RT), to detect any effect(s) of LLPS and opalescence on the
physical stability. As shown in Figures 3A and B, stirring mAb1 samples resulted in a flagrant
turbidity increase in all formulations. We noted that the turbidity in the 0 mM NaCl condition was
less pronounced compared to the other conditions and that the 10- and 22.5- mM NaCl samples
had maintained a mild opalescent appearance throughout the experiment. Interestingly, in our
case, L-arginine HCl did not protect against contact stirring despite its reported role as a
suppressor of protein-surface interactions and aggregation (57). The visibly aggregated samples
were centrifuged for 2 hours at approximately 21.000 g to separate the pellet from the
supernatant. To our surprise, pellets comparable in size were observed in all five different
formulation conditions. Moreover, this revealed that the 10- and 22.5-mM NaCl samples clearly
stayed opalescent after stirring, and that the molecular arrangements responsible for these
phenomena also could sediment to some extent, revealing the presence of a transparent top
dilute phase as observed in the case of mAb network formation (58). This was also the case for
the non-stirred samples (Figure 3B).

We next performed a qualitative assessment of the generated particles by brightfield microscopy
and confirmed that aggregates were formed in all formulations and responsible for the observed
pellet (Figure 3C). It was further observed that their apparent morphologies varied between
formulations, with smaller particles being formed at 0 mM NaCl, relatively larger at 150 mM NaCl
and 10 mM NaCl+150 mM L-arginine HCl, while large, aggregate agglomerates were observed at
10 and 22.5 mM NaCl. Strikingly, droplets were observed in the soluble fraction of the stirred 10

mM NaCl sample, demonstrating that LLPS persists after harsh stirring or is able to reform rapidly thereafter (Figure 3C, bottom). Finally, we calculated the monomer recovery in the different formulations by measuring the concentration in the dilute phase divided by the starting concentration for all samples. Here, we added L-arginine HCl directly to the samples, to avoid non-linear concentration effects from the LLPS/opalescence. Within error, no differences in monomer recovery between the samples were detected, suggesting that the stirring-induced aggregation observed is independent of ionic strength (Figure 3E). Aggregation was observed even after the formulations were supplied with 0.15 mg/mL polysorbate 80 indicating that the observed effect described above does not solely arise from the air-water interphase but also from the bulk solution (Figure S7).

Discussion

In this work we explored the phase behavior of a model therapeutic mAb as a function of formulation-relevant parameters. Specifically, we evaluated the effect of ionic strength over a large drug product relevant concentration range (≈5-70 mg/mL) using a high-throughput combinatorial microfluidic droplet setup (PhaseScan) minimizing time and material requirements (Figure 1D). From this technique, we could rapidly deduce that mAb1 displayed reentrant phase separation, undergoing LLPS at RT, above a critical saturation concentration of 30 mg/mL and in an apparent NaCl range of ≈5-10 mM, after which it returned to its original mixed state, passing through an intermediate, highly opalescent LLPS-free phase. Interestingly, the scattering intensities were not symmetric around the phase border, with higher light scattering intensities measured above the upper critical NaCl concentration compared to the lower boundary, which could be explained by different molecular orientations in solution. Recently, reentrant phase behavior as a function of NaCl was reported for the intrinsically disordered Rabies Virus Phosphoprotein (RABV P) (59). Together with our present study on the multidomain mAb1, these represent two of the few studies showing that monovalent ions can induce reentrant phase transitions in protein systems.

The ability of mAb1 to phase separate at ambient temperature and with a relatively low saturation concentration is uncommon for mAbs. However, a similar case was reported for another mAb, mAb-B, and attributed to a strong enthalpic contribution capable of overcoming the entropic penalty of de-mixing and requiring high temperatures to shift the system toward a homogenously mixed state (60). The sharp response in phase behavior to a slight change in ionic strength suggests that electrostatic interactions are the main drivers of mAb1 LLPS. It is worth mentioning that from the above-mentioned setup alone, we cannot exclude that NaCl partitions into the phase-separated droplets and thereby influences the LLPS thermodynamics. Nevertheless, it can be speculated that in the region below the lower critical NaCl concentration, long-range repulsion is partially screened, enabling attractive short-range interactions, but not to an extent that is conducive to LLPS. Adding a small amount of NaCl might then further screen the long-range Coulomb repulsion between the mAb1 molecules and favor the association through short-ranged interactions into long-range networks leading to LLPS (21). In the vicinity of the upper critical NaCl concentration for LLPS of 10 mM NaCl, samples did not show signs of large-scale self-association but displayed high scattering/opalescence comparable to that of the LLPS region as exemplified here through the 22.5 mM NaCl condition, whose scattering and visual properties are indistinguishable from the phase-separated 10 mM NaCl condition, but is devoid of LLPS (Figure 1). This observation corroborates the relationship between opalescence and proximity to the critical region for LLPS (61, 62). Sequential additions of NaCl up to physiological concentrations decreased the level of self-assembly and returned the scattering intensity to roughly its original value, which is counterintuitive as the association is expected to increase as a result of the reduced Debye length (63). This peculiarity has been observed for several mAbs (6, 25, 29, 31) and has been attributed to the presence of electrostatically complementary patches on their surface (6). Used here as orthogonal techniques to the microfluidic approach mentioned above, quantification of the relative light scattering intensity at 90° as a function of NaCl in conjunction

with optical microscopy confirmed the lower NaCl boundary for LLPS. However, collecting more
data above the apparent upper critical NaCl concentration for LLPS determined with the
combinatorial microfluidic mixing revealed that it extended up to roughly 20 mM for our static
concentration of 45 mg/mL mAb1 (Figure S7). In conclusion, the relationship between mAb
concentration, ionic strength and self-assembly behavior can be highly non-linear and difficult to
extrapolate to other mAb systems (64). However, techniques such as the microfluidic PhaseScan
setup used here, capable of accessing a wide range of the design space integrated with
complementary methods such as light scattering allow us to rapidly and sensitively tell two
macroscopic manifestations of mAb self-assembly and potential developability issues apart:
namely LLPS and high opalescence.
353
In a formulation development context, the characterization of physical stability phenomena linked
to compromised product integrity is crucial to derive tailored mitigation strategies. However, most
biophysical techniques require extensive sample dilution prior to analysis, drastically altering the
physicochemical environment and interaction thermodynamics (65). To circumvent this, we
applied SAXS to provide a quantitative characterization of the interactions involved in LLPS and
opalescence at relevant concentrations. Reports of SAXS used in therapeutic mAb formulation
development are scarce, compared to e.g. dynamic light scattering. However, this highly sensitive
technique offers the advantage of simultaneously reporting on both colloidal and conformational
stabilities and allows for high concentration studies (6, 13, 66, 67). Despite having clearly
distinguishable features when studied by brightfield microscopy, the static SAXS curves for the
LLPS and opalescent conditions were highly similar and characterized by the presence of small
clusters known to arise from a combination of soft long-range electrostatic repulsion and short-
range attraction at low ionic strength (6, 53, 54). This suggests that both phenomena rely on
attractive interactions leading to cluster formation but that the small difference in ionic strength
(10 vs 22.5 mM NaCl) dictates whether they will successfully assemble into a network capable of
large-scale de-mixing or not. This is in line with observations for other mAb systems showing that
increasing the ionic strength disrupts LLPS (25). When evaluated for the LLPS condition, addition
of 150 mM L-arginine HCl led to a higher degree of inhibition of these interactions compared to
increasing the NaCl concentration to 150 mM NaCl. This indicates that the effect of adding L-
arginine HCl is not purely ionic since we observe a difference between the two samples, which
have comparable ionic strengths. Interestingly, despite minimizing the degree of attractive
interactions, the faint correlation peaks for clusters were still visible at these conditions,
suggesting they might still be present but in very low amounts. In this study, we also applied
SAXS coupled to a microfluidic mixing setup to achieve high control of the sample environment
and add a temporal dimension to the analysis. This provides a quantitative characterization of the
interactions involved in the onset and early stages of dynamic processes such as LLPS. In this
time-resolved SAXS setup, the mixing is diffusion-driven, meaning that the relatively slower
migration speed of large mAb1 molecules compared to the small ionic NaCl and buffer
compounds will inevitably generate an inhomogeneous sample environment within the mixing
channel and complicate the discrimination between dilution effects and actual structural
rearrangements (68). Based on this, we rationalized the profile for the structure factor evolution in
our LLPS condition in Figure 2F (pink trace) as follows: at first the mAb1 stock is slowly mixed
with the buffer+NaCl stock solution, thereby approaching the phase border and leading to
increasingly attractive interactions in solution until LLPS is formed, after which the S($\mathbf{q}$) stabilizes
and remains unchanged.
389
In summary, mAb1 displays a peculiar phase behavior characterized by a reentrant phase
transition within a narrow salt range. Just like our LLPS condition (10 mM NaCl), the selected
condition (22.5 mM NaCl) directly flanking the upper critical NaCl concentration for LLPS is
characterized by attractive interactions, the presence of small clusters and a high degree of
opalescence, apparently only differing in the absence of droplets. This implies that the two
phenomena are molecularly distinct and in the case of LLPS, mAbs can assemble into phase-
separating networks when the correct balance of long-range repulsion and short-range attraction

is met. However, a small variation in ionic strength can result in a change in molecular attributes,
resulting in the abrogation of LLPS and conservation of opalescence. SAXS analyses further
reveal that the interactions underlying the LLPS phenomenon occur on the sub second timescale
in solution, which can be specifically inhibited by L-arginine HCl. This technique is also able to
detect potentially problematic residual attractive interactions in a visibly clear sample, which may
guide formulation studies in saving time and valuable resources.
403
Finally, an important aspect of the fundamental study of therapeutic mAb self-association from a
drug development perspective is to link this information to possible repercussions on the physical
stability of the formulations (69). In practice, such studies are laborious and demand substantial
resources (70). Stability studies are therefore complemented by forced degradation studies to
generate a rapid proxy overview of the degradation profile of a drug product (71). This is usually
achieved by subjecting mAb formulations to higher temperatures, shaking, freeze-thaw cycles,
stirring and/or other stress factors (72). For mAbs, stirring represents one of the harshest physical
perturbations and has been shown to rapidly induce the formation of large amounts of aggregates
(73–76). The enhanced destabilizing effect of stirring has been explained by a mechanism in
which the generation of conformationally altered mAbs adsorbed to the solid surface of the
container can be recycled into the bulk solution through abrasion via contact with the stirring bar
(75). In our forced degradation setup, stirring of all formulations produced solid pellets of
comparable sizes, suggesting that its effect is independent of ionic strength in the timeframe
studied. Importantly, LLPS was conserved for the 10 mM NaCl condition, coexisting with solid
aggregates, while the opalescent sample (22.5mM NaCl) only displayed the latter, demonstrating
that the two phenomena have distinct physical stability profiles. This was also the case for
samples containing PS80, suggesting that the bulk solution also contributes to the overall
aggregation, which is in line with the adsorption/abrasion mechanism described above (Figure
S7). The fact that hard centrifugation wasn't enough to completely sediment LLPS droplets in the
10 mM NaCl sample suggests that their volume fraction is small and that there could exist an
equilibrium between them and free, smaller clusters in solution. Finally, the observation that LLPS
and opalescence were unaffected by stirring and that the same amount of mAb material was
converted into aggregates in all formulation points toward the presence of two decoupled
mechanisms. One in which mAb1 self-association is dependent on ionic strength, leading to
cluster formation capable of undergoing LLPS under favorable conditions or remaining dispersed
in solution and result only in opalescence. The other stress-induced mechanism is independent of
ionic strength and hence LLPS/opalescence, resulting in the formation of solid aggregates (Figure
4). Traditionally, LLPS and opalescence have been viewed as precursors of aggregation in mAb
formulations. Here, we report a not so straightforward relation between these phenomena, which
should be taken into consideration during the rational design of mAb formulations. Taken
together, our data demonstrate that mAbs can have a strikingly sensitive response to formulation
parameters, displaying delicate zones of LLPS that are likely to be overlooked. We speculate that
it might be possible to always identify excipient and mAb concentration combinations where LLPS
can be brought to light, as long as one just searches carefully enough.

438
439 **Materials and Methods**
440
441 **Model antibody**
442 The model therapeutic mAb used in this work, mAb1, has a molecular weight ≈150 kDa and a pI
443 ≈8, and was supplied by Novo Nordisk A/S in a proprietary formulation before being stored at -
444 20°C as aliquots.
445
446 **Buffer and stock preparation**
447
A minimalistic buffer containing 10 mM L-histidine was prepared freshly using reagent grade L-
histidine (ReagentPlus®, ≥99% TLC, H8000, Sigma Aldrich) in Milli-Q water with a specific

resistance of 18.2 MΩ/cm at 25°C. The buffering agent was allowed to dissolve on a magnetic
stirrer before the pH was adjusted to pH 6.5 (+/- 0.05) using 1N Hydrochloric acid solution (c(HCl)
= 1 mol/l (1 N), Titripur®, reag. Ph. Eur., reag. USP, 1.09057,1000, Supelco). Sodium chloride
(1.37017.5000, Merck) and L-arginine HCl (EMPROVE® EXPERT, Ph. Eur., ChP, JP, USP,
1.01587, Sigma Aldrich) and polysorbate 80 stocks (1.37171, high purity, EMPROVE® EXPERT,
Ph. Eur., ChP, JP, NF, Sigma Aldrich) were prepared freshly in analysis buffer (10 mM L-histidine
pH 6.5) and filtered through a 0.1 um Whatman Anotop filter (GE Healthcare, Cat no: 6809-2012)
mounted on a silicone free luer lock syringe (Henke Sass Wolf, Henke Ject®, Cat no: 4050-
X00V0) pre-washed according to a previous protocol (77).
459
460 **Buffer exchange by dialysis**
461
462 Dialysis was carried out using Slide-A-Lyzer™ cassettes (Catalog number: A52976, Merck, 20
463 kDa MWCO) in a 10 mM histidine buffer adjusted to pH 6.5. The cassettes were first hydrated in
464 a separate beaker with Milli-Q water before use. The procedure was carried out twice for two
465 hours at room temperature (22°C) and overnight (16 hours) at 4°C using fresh buffer with a
466 volume 500 times larger than the sample volume at each step.
467
468 **Sample preparation**
469
470 All samples were prepared in 10 mM histidine pH 6.5, directly from the freshly dialyzed mAb1
471 stock. Fresh NaCl stocks were used to prepare the different conditions. A 40 mM NaCl stock in
472 10 mM histidine pH 6.5 was used to prepare samples containing 2.5-22.5 mM NaCl, while a 500
473 mM NaCl stock was used for samples containing higher salt.
474
475 **Sample concentration determination**
476
477 Protein concentrations were determined as independent duplicates by measuring the UV-Vis
478 absorbance at 280 nm on a NanoDrop™ One C spectrophotometer. Serial 1:1 dilutions of the
479 stock solution in buffer were prepared from a factor 2 to 64. The absorbance of each dilution was
480 measured using a theoretical molar extinction coefficient at 280 nm and the molecular weight
481 before being multiplied by the dilution factor.
482
483
484 **Right-angle static light scattering**
485
Static light scattering experiments were performed at 90° with a 635 nm semiconductor laser,
using the manual mode interface of the Labbot spectrophotometer (ProbationLabs, Sweden). A
total volume of 400 µl for each sample was transferred to a high precision quartz glass, 10x4 mm
light pathlength cuvette (Catalog number:104F-10-40, Hellma Analytics, Germany).
Measurements were performed on independent duplicate samples, at room temperature (22°C)
that were filtered through a pre-washed 0.1 um Whatman Anotop filter (GE Healthcare, Cat no:
6809-2012) mounted on a silicone free 1 mL luer lock syringe (B. Braun, Injekt®-F Luer Solo, Cat
no: 9166017V).   As soon as the scattering signal stabilized, ten consecutive measurements were
performed before being averaged. The data was normalized to the highest scattering intensity.
495
496 **Brightfield microscopy**
497
498 Brightfield microscopic images were acquired at room temperature (22°C) with a Zeiss Axioscope
499 5 equipped with an Axiocam 305 color camera, through a LD Plan-Neofluar 20x/0.4 objective and
500 processed using ImageJ software (78).
501
502 **Combinatorial microfluidic mixing (PhaseScan)**
503

The phase space of mAb1 as a function of NaCl was mapped out at room tmeperature using
PhaseScan, according to published procedures (21, 45, 79). Pre-defined combinations of
Alexa647 N-hydroxy succinimidyl (NHS) ester labeled mAb1, 10 mM histidine buffer (pH 6.5) and
a 40 mM NaCl stock containing Alexa488 dye were encapsulated in HFE-7500 oil (FluoroChem)
supplied with 1.2% (w/V) fluorosurfactant, (RAN Biotechnologies) by flowing the latter into the
microfluidic device at a constant flowrate. A total of 46581 individual droplets containing pre-
defined aqueous components were evaluated for the presence of LLPS using an inverted
fluorescence microscope (OpenFrame, Cairn Research, Faversham, UK) equipped with a
camera (Kinetix, Photometrics, Tucson, AZ, USA), through a 20x objective. The fluorescence
intensities in the separate channels were used to back calculate the mAb1 and NaCl
concentrations for each droplet.
515
Synchrotron size-exclusion chromatography (SEC)-SAXS for form factor determination

SEC–SAXS experiments were performed at the P12 EMBL BioSAXS beamline, at PETRA III,
EMBL Hamburg, operated at a fixed energy (10 keV, λ = 0.124 nm). The form factor was
determined at room temperature by SEC-SAXS using a Superdex S200 column coupled to an
Agilent 1260 Infinity Bio-Inert high performance liquid chromatography (HPLC) system with an in-
built temperature-controlled auto-sampler. A total volume of 70 µL mAb1 solution at a
concentration of 10 mg/mL in 10 mM histidine pH 6.5+150 mM NaCl was injected into the
column. The same buffer was used as mobile phase, and the flowrate was set to 0.65 mL/min.
SAXS data was collected for the whole column run. The resulting frames were processed using
CHROMIXS from the ATSAS package (80).

Static SAXS

SAXS of mAb1 at 45 mg/mL in 10 mM histidine pH 6.5 containing 10, 22.5 and 150 mM NaCl or
10 mM NaCl+ 150 mM L-arginine HCl was collected at the P12 beamline (PETRA III, DESY
synchrotron, Hamburg), following standard procedures and at room temperature. For each
sample, a buffer-buffer-sample-buffer-buffer measurement strategy was employed, and 50
frames were measured before averaging and buffer subtraction. Finally, the buffer-subtracted
curves were absolute scaled in ATSAS, using a water and empty capillary measurements
performed under the same conditions.(81). The structure factor S($\mathbf{q}$) was obtained by dividing the
scaled subtracted scattering curve with the form factor.

Time-resolved solution SAXS

Time-resolved solution small-angle X-ray scattering was collected at the CoSAXS beamline at the
MAX IV Laboratory, using a microfluidic sample delivery system. A detailed description of the
technical design can be found elsewhere (68). Briefly, the sample is constantly flowing through a
T shaped microfluidic-chip, with three inlets (cyclo-olefin copolymer COC/TOPAS®, 300x400 µm
cross-section, Microfluidic ChipShop). Two out the three available inlets on the microfluidic chip,
contained a dilution of the freshly dialyzed mAb stock, while the last inlet in the middle position
was supplied with either fresh buffer or freshly prepared excipient (NaCl and/or L-Arginine HCl)
stocks. At the mixing point on the microfluidic chip, the mAb is diluted by a factor of 2/3 (i.e. 45
mg/mL) and the excipients, by a factor of 1/3. SAXS data was collected at two of the inlets prior to
mixing, the mixing point and 21 positions from the mixing point at a total flowrate of 60 µL/min as
the chip was translated along $\mathbf{z}$. The time resolution of the experiment was determined by a
combination of the flowrate and the distance at which SAXS was measured from the mixing point.
SAXS data were recorded with an incident X-ray beam of wavelength λ = 0.99 Å, with a sample-
to-detector (Eiger2 X 4m) distance of 3.5 m yielding a q-range of 0.004 < $\mathbf{q}$ < 0.3 Å^{-1}. For each
sample, the background of each inlet was measured prior to replacing the contents of the inlet 1
and 3 with mAb solution. A total of 40 frames were recorded at each point for a total of 50 ms and
averaged, provided that they were of sufficiently good quality before being buffer subtracted. The
scattering curves were then absolute scaled using water and empty capillary measurements

performed under the same conditions as standards. All processing was performed using the
Primus package in the ATSAS data analysis software (81) and the structure factors were
calculated as described in the previous section.

Stirring stress protocol
558
Selected mAb formulations were prepared as 1 mL solutions of 45 mg/mL mAb1. For the stirring
study, 1 mL samples were filtered through a pre-washed 0.1 um Whatman Anotop filter (GE
Healthcare, Cat no: 6809-2012) mounted on a silicone free 1 mL luer lock syringe (B. Braun,
Injekt®-F Luer Solo, Cat no: 9166017V). and two aliquots of 500 µL were filled into separate 4
mL glass screw vials (45X15 mm, MD Scientific, VF013-1545) with a 5x2 mm cylindrical PFTE-
coated stirring bar (BOLA, C 350-03). The vials were capped (Thermo Scientific, B7815-13) and
sealed (Parafilm) before being placed vertically on a magnetic stirring plate (IKA RO 15) and
stirred at 1000 rpm overnight (18h). Aliquots of the samples before stirring were diluted 10 times
in 150 mM L-arginine HCl in 10 mM histidine pH 6.5 and their concentration measured.
568
569   **Monomer recovery after stirring**
570
After stirring, 2M L-arginine HCl in 10 mM histidine pH 6.5 was added directly to the vials to reach
a final concentration of 150 mM. The vials were gently swirled and 400 µL aliquots were
transferred to microcentrifuge tubes before 2 hours centrifugation at approximately 21000 g.
Aliquots of the sample supernatants after stirring and centrifugation were diluted 10 times in 150
mM L-arginine HCl in 10 mM histidine pH 6.5 and their concentration measured, before being
divided by the initial sample concentration (see previous section) to obtain what we called the
monomer recovery here.
578
579
580   **Acknowledgments**
581

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791
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Figures

Figure 1. Phase behavior of mAb1 (A) Visual appearance and (B) normalized right-angle scattering intensities at 635 nm of 45 mg/mL mAb1 solutions as a function of NaCl (0-150 mM), where the NaCl concentrations selected for microscopy are highlighted in blue, pink, purple and green. The experiments were independently performed n=2 times and errors represent standard deviations of the duplicate measurements. (C) Brightfield microscopy images of selected conditions (0, 10, 22.5 and 150 mM NaCl, 20 µm scalebar). (D) Liquid-liquid coexistence curve of mAb1 versus NaCl concentration, evaluated by a combinatorial microfluidic mixing setup with fluorescence microscopy-based LLPS detection. The resulting grid-map was achieved by binning the n = 46581 individual data points (Figure S2) to evaluate the local average phase separation probability (LLPS probability = 1: red, 0.5: white, 0: blue), as described in (79). The insets with red and blue borders show representative microscopy images of phase-separated mAb1 inside the mAb1/buffer/NaCl in oil microemulsion droplets and one with no detected LLPS, respectively.

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Figure 2. Characterization of interactions underlying mAb1 LLPS with SAXS (A) Structure
factor measured for 45 mg/mL mAb1 + 10 mM NaCl, 22.5 mM NaCl, 10 mM NaCl + 150 L-
arginine HCl (called 10 mM NaCl+Arg here) and 150 mM NaCl, from static SAXS experiments (B)
Schematic representation of the microfluidic chip coupled to the Co-SAXS beamline. (C)-(E)
Time-resolved SAXS data of 45 mg/mL + (C) 10 mM NaCl, (D) 10 mM NaCl + 150 mM L-arginine
HCl and (E) 150 mM NaCl recorded at 22 distances from the mixing point across the channel.
The distances were converted to timepoints here. Data was recorded at a total flowrate of 60

µL/min (F) Average and associated standard deviations of the first three S(**q**) values for each
timepoint of the time-resolved SAXS data as a function of time from the mixing point.
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Figure 3. Physical stability of mAb1 samples as a result of stirring stress. Visual appearance of 45 mg/mL mAb1 solutions in 10 mM histidine pH 6.5 at 0, 10, 22.5, 150 mM NaCl or 10 mM NaCl+150 mM L-arginine HCl (10 mM NaCl+Arg) before (A) and after (B) magnetic stirring overnight (approximately 18 hours) at 1000 rpm and subsequent centrifugation at approximately 21000 *g* for 2 hours at RT. (C) Brightfield microscopy of the stirred samples and the supernatant after centrifugation (50 μm scalebar). (D) Representative images of the stirred and centrifuged samples with added L-arginine HCl. Samples were prepared at a larger volume for the images, for increased clarity (E) Monomer recovery of the different conditions, measured on two independent samples. The numbers on the individual bars represent the calculated monomer recovery, where 1 and 0 stand for complete and no monomer recovery, respectively. Errors represent standard deviations from duplicate measurements.

Figure 4: Summary of mAb self-assembly behavior at 45 mg/mL, as a function of NaCl concentration and applied stirring stress. mAb1 LLPS and opalescence occur in a narrow NaCl range and can be inhibited by L-arginine HCl. Solid aggregation is decoupled from LLPS and opalescence. LLPS and opalescence are unaffected by stirring induced stress.

Supporting Information for

Decoupling liquid-liquid phase separation and opalescence from stress-induced aggregation in therapeutic mAb formulations

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This file includes:

Figures S1 to S7

Figure S1: mAb1 LLPS is liquid-like (A) Coalescence of droplets, as indicated by the white arrowhead (10 μm scalebar). (B) Wetting of the glass surface of the microscopy slide over time (100 μm scalebar)

Figure S2: Coexistence curve of mAb1 as a function of NaCl determined using combinatorial microfluidics. Each of the 46581 observations is shaded according to phase separation probability based on local radial averaging. An eye guide for the approximate location of the binodal is indicated by the dashed black line.

Figure S3: Selected dense phase morphologies detected with PhaseScan using fluorescence microscopy (20 µm scalebar)

Figure S3: Overview of SEC SAXS measurements of mAb1 (A) Elution profile of 10 mg/mL mAb1 in 10 mM histidine pH 6.5 + 150 mM NaCl mobile phase showing the average integrated SAXS intensity I(q) ($1.48{*}10^{-3}$ Å^{-1} < q < 0.556 Å^{-1}) as a function of frame number (B) Average scattering curve of frames **Figure S3 (continued):** 1454 to 1521, corresponding to monomeric mAb1 (highest peak of the elution profile in A) (C)

Dimensionless Kratky plot showing three peaks, as expected for IgG molecules (D)
Guinier plot for the monodisperse mAb1 sample showing linearity in the Guinier range
and the radius of gyration determined from the slope.

Figure S4: Suppression of LLPS and opalescence with L-arginine HCl and effect of
stirring the latter (A) Visual appearance of an LLPS sample containing 45 mg/mL
mAb1 in 10 mM histidine, 10 mM NaCl, pH 6.5 compared to 45 mg/mL mAb1 in 10 mM
histidine, 10 mM NaCl, 150 mM L-arginine-HCl, pH 6.5 (10 mM NaCl+Arg). The latter
was added prior to adding the NaCl that would have otherwise made the sample
undergo LLPS (left) Brightfield microscopy of the 10 mM NaCl+Arg sample showing that
no LLPS is detected under these conditions. The scalebar represents 50 µm. (B) Same
setup as in (A) but with the 22.5 mM (opalescent sample) as well as images of the effect
of stirring at 1000 rpm overnight (18 hours), showing the increased visual turbidity of the
sample and the presence of aggregates in the microscopy image.

Figure S5: Overlay of the scattering curves (intensity I(q) vs q) for the last timepoint in the time resolved SAXS experiments (black curves) and scattering curves from the static SAXS experiment (colored curves) for 45 mg/mL mAb1 in 10 mM histidine pH 6.5 containing 10 mM NaCl (A), 150 mM NaCl (B) or 10 mM NaCl + 150 mM arginine HCl (C)

947 **Figure S6: Phase boundary of mAb1 as a function of NaCl determined with optical**
948 **microscopy.** Brightfield microscopy of 45 mg/mL mAb1 in 10 mM histidine pH 6.5 at
949 room temperature as a function of NaCl concentration (0, 2.5, 5, 7.5, 10, 12.5, 15, 17.5,
950 20, 22.5, 25, 50, 75, 100, 125, 150 mM) with LLPS region highlighted in pink. The
951 scalebar represents 50 µm.

Figure S7: Effect of PS80 on the stirring induced aggregation (A) Visual appearance
and brightfield microscopy images of 45 mg/mL mAb1 in 10 mM histidine pH 6.5
containing 10 (A) or 22.5 (B) mM NaCl with 0.15 mg/mL PS80 added. The left images
are before stirring and the images on the right are after overnight stirring as described in
the Materials and Methods section. The scalebar represents 50 μm in the main
microscopy image and 10 μm in the inset zoom image. In the 10 mM NaCl + 0.15 mg/mL
PS80 images, the difference in droplet size arises from their fast dynamics and
difference in times at which the images were acquired.