Systemic inflammation reduces astrocyte Ca^{2+} and neurovascular coupling in a mouse model of Alzheimer's disease

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ABSTRACT

Neuroinflammation and neurovascular dysfunction are two major pathologies in Alzheimer's disease (AD), yet their interplay remains poorly understood. Astrocytes are central players in both brain immunity and neurovascular coupling. In this study, we induced neuroinflammation through systemic administration of lipopolysaccharide (LPS) in 12-month-old APP/PS1dE9 mice and simultaneously monitored the astrocyte Ca^{2+} signaling and the brain hemodynamics with two-photon microscopy. We showed that the spontaneous release of Ca^{2+} in astrocytes was elevated in AD mice and decreased by 14 days of LPS administration. The effects of LPS-induced inflammation on astrocytic Ca^{2+} signaling varied substantially between brief 3 sensory stimulation and sustained 30 second sensory stimulation with modest effects on vascular responses. These findings highlight the nuanced impact of neuroinflammation on astrocytic Ca^{2+} dynamics and brain hemodynamics in AD, shedding light on mechanisms that link these pathologies.

Keywords: Alzheimer's disease, neuroinflammation, lipopolysaccharide, astrocyte Ca^{2+}, neurovascular coupling, two-photon microscopy

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1. INTRODUCTION

Neuroinflammation and neurovascular dysfunction are two major pathologies in Alzheimer's disease (AD) [1–4]. These pathologies share cellular components, with astrocytes playing a vital role in both brain immunity and neurovascular coupling [5,6]. Under inflammatory conditions, astrocytes become activated, undergoing phenotypic and morphological changes that facilitate the release of cytokines. The reactive astrocytes contribute to amyloid beta pathology and neural network dysfunction [7,8]. Studies showed altered astrocyte Ca^{2+} signaling in reactive astrocytes [9,10]. Additionally, astrocyte Ca^{2+} signaling also regulates cerebral blood flow [6]. Thus, investigating astrocytic Ca^{2+} signaling and cerebrovascular function under inflammatory conditions will provide insights into the relationship between neuroinflammation and neurovascular dysfunction in Alzheimer's disease. Previous studies showed systemic inflammation disrupts cerebral hemodynamics in healthy rodent brains and human patients with small vessel disease and traumatic brain injury [11–13]. Systemic injection of the bacteria-derived endotoxin lipopolysaccharide (LPS) has been used as a model to study neuroinflammation in neurodegenerative disease [14]. Peripheral inflammation induced by systemic injection of LPS can transfer to the central nervous system and cause a prolonged inflammatory response in the brain [15]. Here, we subjected the 12-month-old female APPswe/PS1dE9 mice and their wildtype littermates (n=8 each) to two weeks of LPS-induced systemic inflammatory threat and measured cerebral vessel dynamics and astrocyte Ca^{2+} release during functional brain activation using two-photon microscopy.

2. METHODS

2.1 Animal preparation

All experiments were performed following ARRIVE guidelines for animal care, under a protocol approved by the Northeastern University Institutional Animal Care and Use Committee. The mouse strain used for this research project, B6C3-Tg(APPswe,PSEN1dE9)85Dbo/Mmjax, RRID:MMRRC_034829-JAX, was obtained from the Mutant Mouse Resource and Research Center (MMRRC) at The Jackson Laboratory, an NIH-funded strain repository, and was donated to the MMRRC by David Borchelt, Ph.D., McKnight Brain Institute, University of Florida. The double transgenic AD mouse co-expresses the Swedish mutation of amyloid precursor protein (APP) and a mutant human presenilin 1 gene (PS1-dE9) and accumulates beta-amyloid deposits in the cortex at 6 months [Jankowski 2004]. The study used female APP/PS1dE9 mice and their wild-type littermates (age 12-13 months, n=8 per cohort) [1]. At 10 months of age, mice underwent cranial window surgery followed by GFAP-promoted GCaMP6f virus injection. Under isoflurane anesthesia (3–3.5%

isoflurane for induction and 1–2% for maintenance), hair and skin was removed to expose the skull, and a titanium butterfly-shaped head post was implanted using dental cement [17]. After the localization of the injection site, a ~ 3 mm diameter of cranial window was created on the barrel cortex of the mouse, followed by targeted injection of a GFAP-promoted GCaMP6f virus (pZac2.1gfaABC1D-cyto-GCaMP6f, Plasmid #52925, Addgene). Virus (300–500 nL) was injected at 2 nL/s, 300–350 μm below the brain surface, using a glass micropipette and a Nanoinjector III (Drummond Scientific) [18]. Injections were performed in two to three cortical regions to increase the area of viral expression. The procedure lasted 15 to 20 minutes, with the dura kept hydrated throughout. After the injections, the dura was covered with a CNC-machined transparent acrylic coverslip (outer diameter: 5 mm, inner diameter: 3 mm). The mouse was then removed from the stereotaxic frame and allowed to recover from anesthesia. The animal was single-housed and provided with 5 days of post-operative care (40/8 mg/ml, sulfametoxazole/trimethiporim (SMX-TMP) in drinking water). Buprenorphine (0.05 mg/kg at 0.03 mg/ml) was administered subcutaneously for three days after surgery. To label astrocytes in the activation center, we conducted optical intrinsic signal imaging (OISI) and whisker stimulation on the anesthetized mouse before removing the skull. The skull over the barrel cortex (A-P: 2mm, M-L: 3 mm) was thinned, and whiskers on the contralateral side of the thinned skull were deflected using a cotton swab. The skull was illuminated with an LED light source during the stimulation through a green bandpass filter (568/10 nm). The reflected light was recorded with a CMOS camera (Basler acA1300–$200\mu m$, Edmund optics) mounted on the surgical microscope, and the relative intensity change was calculated with a customized MATLAB script. Regions with the greatest intensity drop were identified as the activation area and selected as the site for viral injection.

2.2 Habituation training

Headpost restraint training started 7 to 10 days post-surgery using a custom-made imaging cradle. During training, the mouse was conditioned to tolerate head immobilization from 5 minutes to 1 hour. Whisker stimulation was included during the final training sessions to acclimate the animal to the functional activation experiment. Milk was given as a reward during the training.

2.3 Systemic inflammation induction

Systemic inflammation was induced through daily intraperitoneal (i.p.) injections of 0.3 mg/kg lipopolysaccharide (LPS, *E. coli* O55: B5, L4005, CAS-No. 93572-42-0, Sigma-Aldrich) for 14 days. A stock solution of LPS was prepared at 1mg/mL in phosphate-buffered saline (PBS) and stored at -20°C. The solution was vortexed and diluted 4-fold to 0.25 mg/mL for each injection.

2.4 Functional activation protocol

A capillary tube with a 3D-printed broom-like end was positioned approximately 2.5–3 cm from the nose, parallel to the right side of the mouse's face, and below the eye to avoid directing air toward the eyes during stimulation. Air puffs were delivered through the tube and controlled using a pneumatic drug injection system (PDES-DXH, ALA Scientific, USA). Two whisker stimulation protocols—brief and prolonged—were performed. The brief protocol consisted of a 5-second baseline, 2.7 seconds of 1.67 Hz stimulation (5 pulses, 20 psi), and 22.3 seconds of recovery. The prolonged protocol included a 5-second baseline, 30 seconds of 1.67 Hz stimulation (50 pulses, 20 psi), and 30 seconds of recovery. Short and long stimulations were interleaved within each trial and repeated 10 times.

2.5 Functional activation center mapping

The activation center of whisker stimulation was mapped using optical intrinsic signal imaging (OISI) under the brief whisker stimulation protocol. A white LED illuminator (SCHOTT KL 1600) with a 568/10 nm bandpass filter (Edmund Optics) served as the light source. The camera was triggered by a TTL signal from a general-purpose input/output (GPIO) hardware trigger. A fiber-optic LED light source illuminator (SCHOTT KL 1600 LED) delivered light to the cranial window at a 60° angle. Reflected light was collected using a 4× objective (Nikon Instruments Inc.) and recorded at 5 Hz for 20 seconds with a CMOS camera (Basler acA1300–200μm, Edmund Optics). Baseline intensity (I_0) was calculated by averaging the intensity over the baseline recording. Relative intensity (I/I_0) was calculated for all imaging frames. Cortical area with the maximal intensity decreases was identified as the activation center.

2.6 Two-photon imaging in awake mice

Two-photon imaging of astrocyte Ca^{2+} signaling and vascular dynamics at barrel cortex at resting-state and during functional activation was conducted using the multiphoton imaging system Ultima2pPlus (Bruker Nano, Inc) with a 25× objective (1.10 NA, Nikon Instruments Inc). Imaging during the functional activation experiment was synchronized with the whisker stimulation protocol. Blood vessels were labeled through retro-orbital injection of Texas Red Dextran (2.5% w/v, 80uL). A tunable ultrafast laser (InSight X3+, Spectral-Physics) was tuned to 940 nm for simultaneous imaging of blood vessels and astrocytic Ca^{2+} imaging. We tracked the penetrating arterioles from the pial surface to the deepest assessable cortical layer and recorded the vessel diameter and the astrocyte Ca^{2+} release using a minimal frame rate of 4.3 Hz. The image field of view (FOV) was around $88 \times 88\ um^2$. On the following day, capillary diameter and red blood cell velocity in response to the interleaved functional activation was measured with two-photon line scanning [19], with a scan frequency ranging from 369.87 to 1034.8 Hz. Angiogram and z-stacks of GCaMP6f-expressing astrocytes (0–350 μm below the pial surface) were taken at the end of the experiment. Penetrating arterioles perpendicular to

the image plane and capillaries parallel to it were selected to ensure accurate diameter estimation, while tilted

vessels were excluded during post-processing. We measured regions from 49 to 414 μm below the pial surface

for WT mice and 30 to 360 μm below the pial surface for AD mice.

2.7 Two-photon imaging data analysis

Astrocyte Ca^{2+}: Image frames were pre-processed using a non-rigid motion correction algorithm [20], followed

by median filtering. Resting-state astrocyte Ca^{2+} fluctuations were quantified using a region-of-interest-based

Ca^{2+} analysis tool: "GECIquant" in ImageJ [21]. Briefly, average intensity projection was generated from the

time series of two-photon raster scan images. We created a binary region of interest (ROI) mask where the area

within the polygon ROI is set to 1 and the rest of the image is set to 0. Mean intensity within the ROI over time

was calculated. The area criterion was set to 30 μm^2 to Inf for astrocyte soma and endfeet, and 8 to 2000 μm^2

for Ca^{2+} waves in processes. Relative intensity change ($\Delta F/F_0 = (F_t - F_0)/F_0 \times 100$) was calculated. F_0

was calculated as the median of the lowest 5% fluorescence intensity over the entire 10-minute raster scan.

$\Delta F/F_0$ of all astrocyte ROIs from all mice were interpolated with a $dt = 0.2244\ s$, (i.e., 4.45 fps). The $\Delta F/F_0$

traces were pre-processed using linear detrending to remove intensity drift that occurred during the

measurement. The detrended intensity traces were then low pass filtered with a cutoff frequency of 0.1 Hz, as

determined by power spectrum analysis. To determine the threshold for the Ca^{2+} event, we reviewed our data

and found that the frequency of Ca^{2+} events within all three astrocyte ROIs (soma, endfeet, and process) is less

than one event per min per ROI. Assuming each event lasted 10 seconds, more than 80% of the 10-minute

recording were 'eventless'. Therefore, we calculated the median absolute deviation (MAD) of the lowest 80%

of the $\Delta F/F_0$ trace and used 5 times the MAD as the threshold for the Ca^{2+} event. This threshold is more robust

to outliers compared to the conventional standard deviation approach and reduces the number of 'false

positives'. Ca^{2+} events were detected and quantified using the 'findpeaks' function in MATLAB. The detected

events were categorized as either 'singlepeak' or 'multipeak' events as described [22]. Finally, we calculated

the frequency of the event as per min per ROI. Ca^{2+} release during whisker stimulation was quantified as $\Delta F/F_0$.

F_0 was calculated as the average intensity during the first 5 seconds of the resting-state recording.

Arteriole diameter: Arteriole diameter in response to functional activation was quantified using the automatic

structure tracking algorithm developed by Haidey et al. [23]. The algorithm tracks the cross-sectional area of

the vessel based on user-defined luminal edges. Vessel diameter (D) was calculated from the cross-sectional

area. Relative change of diameter ($\Delta D/D_0 = (D_t - D_0)/D_0 \times 100$) was calculated, where the baseline

diameter (D_0) was the average diameter over the 5-second resting-state measurement. Since the frame rates of

different imaging fields can sometimes vary slightly, $\Delta D/D_0$ were interpolated with $\Delta t = 0.2244\ s$.

$\Delta D/D_0$, $\Delta F/F$ quantification: We first quantified response in penetrating arteriole (p.a.) and the Ca^{2+} release

in astrocyte endfeet wrapped around the p.a. Stimulation trials were categorized into four groups: (1) trials with

both arteriole dilation and astrocyte endfeet Ca^{2+} increase, (2) trials with only arteriole dilation, (3) trials with

only astrocyte endfeet Ca^{2+} release, and (4) trials with no response in either. Trials with motion artifacts were

excluded. To analyze the correlation between arteriole dilation and astrocyte endfeet Ca^{2+}, we calculated the

average arteriole dilation and Ca^{2+} release in trials where both responses were observed. The averaged arteriole

dilation and Ca^{2+} release were then low-pass filtered with a cutoff frequency of 0.2Hz. Amplitude and kinetics

of the vascular response and Ca^{2+} release were characterized using the 'findpeaks' function in MATLAB. For

30s whisker stimulation, we also evaluate the average response during the last 2s of the stimulation. Average

Ca^{2+} signaling in astrocyte soma and processed were calculated over the selected stimulation trials.

Capillary diameter: Space-time images from two-photon line scans were denoised using a 2D median filter.

Vessel diameter was calculated using the MATLAB two-photon imaging analysis toolbox, CHIPS [24]. The

algorithm normalizes the vessel's intensity profile to a range of 0 to 1 and calculates the diameter using the full

width at a user-defined height. We used the full width at 0.4 of the maximum intensity, as it provided the most

accurate diameter estimation based on our signal-to-background ratio. The sampling rate was set at a maximum

of 20 Hz. Measurements affected by motion, particularly along the axial axis were discarded. The average

diameter and $\Delta D/D_0$ across all selected stimulation trials were calculated. The $\Delta D/D_0$ traces were smoothed

using a moving median filter with a one-second window (20 data points). Vascular dilation amplitude and

kinetics were analyzed using the same method as in raster-scan data analysis. Vessels were categorized by

branch order: 0th-order penetrating arterioles, 1st and 2nd-order capillaries, and higher-order capillaries (3rd-order

branches and above).

Capillary RBC velocity: The space-time images were filtered using Sobel filtering, and the capillary red blood

cell (RBC) velocity was analyzed using the iterative Radon Transform [25]. Image segments of every 100 lines

were used to calculate RBC velocity, velocity at the next time point was calculated after skipping 25 lines.

$\Delta v/v_0$ was calculated and smoothed using a moving median filter.

2.8 Tissue collection and immunofluorescence imaging (IF)

After 14 days of LPS treatment, mice were sacrificed, and brains were collected for immunofluorescence (IF)

staining. IF staining was performed on a subset of the imaged mice (n=3 per cohort). Mice received 14 days of

saline injections at a volume equivalent to the LPS dose of 0.3 mg/kg served as control group (n=2 for WT,

n=3 for AD). Mice were intracardially perfused with 40 mL of heparin-PBS solution, followed by 20 mL of

4% paraformaldehyde (PFA) for fixation. The brains were collected and stored in 4% PFA for a maximum of

24 hours, then transferred to 70% ethanol and stored in $-4\,℃$. The brain samples were sent to the Dana-

Farber/Harvard Cancer Center Specialized Histopathology Services Core (Boston, MA, USA) for

immunofluorescence staining. The samples were paraffin-embedded and sliced into approximately 10 μm thick

sections for IF staining. Nuclei were stained with DAPI, microglia with an anti-Iba-1 antibody labeled with

Alexa Fluor 594, and astrocytes with an anti-GFAP antibody labeled with Alexa Fluor 647. IF images were

collected with confocal microscopy (LSM 800, ZEISS). DAPI, AF-647, and AF-594 were excited with 405nm,

640nm, and 561nm, respectively. Images were taken using $5\times$ and $10\times$ objectives. Barrel cortex and

hippocampus were identified using the Allen Brain Atlas. For each 10× field of view ($638 \times 638\ um^2$), Z-

stack images were collected with a step size of $0.34\ \mu m$. All images were acquired using consistent excitation

power and emission detector gain settings. $A\beta_{1-42}$ was stained with anti-$A\beta_{1-42}$ antibody conjugated to Alexa

Fluor 647. Fluorescence images of $A\beta_{1-42}$ were acquired with wide-field fluorescence microscopy (Zeiss Axio

Observer). All images were acquired using a consistent exposure time.

2.9 IF imaging quantification

GFAP and Iba-1 expression were quantified using the maximum intensity projection (MIP) of the z-series

images. Background was removed and MIP images were binarized using an intensity threshold. The percentage

area of pixels with intensity above the intensity threshold was calculated. Similarly, percentage area of $A\beta_{1-42}$

load in cortex and hippocampus was quantified in Image J.

2.10 Statistical analysis

We performed statistical tests to see if there is difference in baseline astrocyte Ca2+ dynamics, stimulus-evoked

vessel dilation and astrocyte Ca2+ release in AD, and how LPS affect these parameters in both WT and AD

cohorts. Differences between WT and AD group before LPS injection were tested using the Wilcoxon rank

sum test. Effect of LPS on both cohorts were tested using linear mixed effect model with the 'lme4' package

in RStudio. Time (i.e., day0, day 7 and day14) was set as the fixed effect. And the initial value, i.e., parameter

measured at day 0 of each subject were set as the random effect. Pair-wise comparison was conducted with

Tukey's method in the 'emmeans' package. * = p<0.05, ** = p<0.01, ***=p<0.001, ****=p<0.0001.

3. RESULTS

Among its many functions, astrocyte Ca2+ is an important mediator of neurovascular coupling [6]. Previous studies reported activated astrocytes and increased astrocyte spontaneous release of Ca2+ in the APPswe/PS1dE9 mice cortex. To determine whether astrogliosis affects astrocyte Ca2+-mediated contributions to cerebral blood flow regulation, we measured astrocyte Ca2+ dynamics and microvascular dilation under resting-state conditions and during functional hyperemia in the awake APPswe/PS1dE9 mice brain at age 12- to 13-months. We then explored if a 14-day LPS-induced neuroinflammation challenge alters astrocyte calcium signaling and its contributions to neurovascular coupling.

Recent studies demonstrate that astrocyte Ca2+ contributes significantly to sustaining functional hyperemia in response to prolonged, but not brief, periods of cortical stimulation [26]. Motivated by these findings, we used two-photon imaging to measure brain hemodynamics and astrocyte Ca2+ release in response to both brief (3s) and sustained (30s) whisker stimulation.

Measurements were performed in cortical layers I and IV. Analysis via linear mixed effects model revealed no significant differences between cortical layers. As a result, the data from both layers were combined.

3.1 Pre-inflammation: Hyperactive astrocytes and reduced stimulus-evoked astrocyte Ca2+ in AD mice

We first evaluated resting-state spontaneous cortical astrocyte Ca2+ by imaging GCaMP6f-labelled astrocytes in awake mice. Raster scanning was performed in ~88 μm cortical regions surrounding penetrating arterioles for 10 min at ~ 4.4 Hz. Dynamic Ca2+ transients were quantified and analyzed from the soma, processes, and endfoot compartments of astrocytes. In AD mice, we observed ~15 – 40% higher frequencies of Ca^{2+} spikes compared to age-matched wildtype littermates, with significantly higher Ca2+ frequency in the soma and process compartments (Fig. 1B-C, left, p-val = 0.03 soma, p-val = 0.048 processes). No differences in the Ca2+ amplitudes were observed between AD and WT mice. Compared to WT littermates, the mean duration of the astrocytic Ca2+ spikes in AD mice was significantly lower (26 %, p-val < 1e-4) in astrocyte processes. Shorter Ca2+ durations were also observed in the soma and endfoot compartments in AD mice; however, the differences were not significant. (Fig. 1C).

Next, we investigated whether amyloid pathology impacts functional hyperemia. We first applied optical intrinsic signal imaging (OISI) during a 3 s whisker stimulus to locate the activation center (fig 1.D). We measured astrocyte Ca2+ dynamics and diameter of penetrating arterioles while stimulating the mouse barrel cortex via pneumatic whisker deflection. Our OISI measurement revealed slight, but not significant, differences

in peak cerebral blood volume response (< -1%) in AD mice relative to WT (Fig. 1C). The activated region

was then imaged via TPM using both raster scanning (4.4 Hz, fig 1.E) and rapid line scanning (~360 – 100 Hz,

downsampled to 20 Hz).

In response to a short ~3s functional stimulus, AD and WT mice demonstrated different responses for arterial

dilation and $Ca2^+$ signaling within astrocyte compartments. In WT mice, the area under the curve (AUC) for

arterial dilation response was significantly higher in WT mice (40% difference, p = 0.029), while arterial peak

dilation, rise times, and latency were similar between cohorts (Fig.1F and supplementary figure 1). Astrocyte

Ca2+ kinetics vary in different cell compartments, as reported previously. Peak amplitudes of stimulus-induced

Ca2+ release in AD mice appeared higher in all astrocyte compartments compared to WT mice; however, the

differences were not statistically significant (Fig. 1 G-I, soma p = 0.23, endfeet p = 0.21, processes p= 0.054).

AD mice demonstrated significantly shorter Ca^{2+} responses in astrocytic endfeet (supplementary figure 1, p =

7e-4). In both cohorts, we consistently observed that the short 3s whisker stimulus evoked slower astrocyte

Ca2+ responses relative to the vascular response. Arterioles dilated to their maximum approximately 2,1

seconds after the stimulus onset, while all astrocyte Ca2+ responses achieved their maximal values

approximately 1-1.5 s after stimulus cessation. While the slower response times in astrocytes support earlier

studies that downplay contributions of astrocyte Ca2+ to neurovascular coupling, our results indicate that

indicate astrocytes in the AD mice brain respond slightly faster and more pronouncedly than WT mice to a

brief sensory stimulus.

A longer 30s whisker stimulus yielded more striking differences between AD and WT mice, particularly in

astrocyte Ca2+ dynamics. Response profiles exhibited biphasic features for both arterial dilation and astrocyte

Ca2+ release - including a rapid rising phase followed by a prolonged plateau phase. Consequently, we analyzed

dilation and Ca2+ release both over the full stimulus duration (all 30 seconds) as well as the late phase (the

final 2 seconds). Again, AD and WT mice experienced comparable peak diameter in arterioles. Following peak

dilation, arterioles constricted slightly and plateaued to a slightly smaller diameter (Fig. 1 J). For both phases

of the 30s stimulus, we observed no significant differences in arterial dilation rise times, maximal diameter, or

AUC between AD and WT mice. However, following stimulus cessation, we observed significantly faster

constriction to baseline diameter in AD mice (supplementary Figure 1, Δt = 5.04s, p = 0.03). Astrocyte Ca2+

responses differed more substantially between cohorts for the 30 s stimulus (Fig 1 K-M). In WT mice, astrocytes

persistently release Ca2+ from all compartments until the stimulus cessation, while Ca2+ release in AD

astrocyte peaked rapidly during the first ~5s of stimulation and diminished significantly during the later ~25s.

Although lower Ca2+ was observed within all astrocytic compartments in AD mice, the most pronounced and

significant differences were observed in astrocyte processes (Fig. 1 M & Supplementary Figure 1, p < 1e-4).

During the final 2s of the stimulus, peak Ca2+ release was significantly lower in AD mice relative to WT mice

for all astrocyte compartments (Fig.s1 J-M, soma p = 1e-4, endfeet p = 7e-4, processes p < 1e-4). Our

observations indicate a compartmentalized influence of AD pathology to astrocyte Ca2+.

To examine how amyloid pathology and associated hyperactive astrocytes affects hemodynamics in smaller

vessels, we performed rapid two-photon line scan measurements to measure capillary diameter and red blood

cell speed. Vessel diameter was downsampled to a rate of 20Hz. Vessel dilation in laterally-oriented arteriole

branches and capillary branches extending from the downward penetrating arteriole (1st order to 4th order) were

measured. We found significant differences in stimulus-induced arteriole dilation between AD and WT mice

in response to 3 second stimulus. In capillaries, we observed no differences in dilation between AD and WT

for either stimulus duration (supplementary Figure 1).

Figure 1. Spontaneous astrocyte Ca2+ and sustained sensory stimulation in AD and WT mice barrel cortex.
(A) 2D, raster scan image showing vasculature labelled with Texas-Red and astrocytes expressing GCaMP6f.
Annotated regions are soma (red), endfeet (blue), and process (magenta). **(B)** Representative measurements of
spontaneous Ca^{2+} release in cortical astrocytes cell compartments recorded for 10 mins. **(C)** Amplitude, Frequency
and Duration of Ca^{2+} spikes at different astrocyte ROIs. **(D)** OISI measurement of cerebral hemodynamics in response
to 3s whisker stimulation in left barrel cortex in WT and AD mice. **(E)** Representative two-photon raster scan images
of diving arteriole dilation and astrocyte Ca^{2+} release during whisker stimulation trials. **(F-I):** Trial-averaged profiles
of arteriole dilation and astrocyte Ca^{2+} release in response to 3s whisker stimulation and quantification of the peak
response. **(J-L):** Trial-averaged profiles of arteriole dilation and astrocyte Ca^{2+} release in response to 30s whisker

stimulation and the quantification of the peak response. Difference between WT and AD were tested using rank-sum
test.

3.2 LPS-induced inflammation reduces spontaneous astrocyte Ca2+ and impairs neurovascular coupling

To evaluate how systemic inflammation alters astrocyte's Ca2+ signaling and its contributions to CBF
regulation, animals underwent a prolonged 14-day LPS-induced inflammation challenge. We used 2-photon
imaging to measure astrocyte Ca2+ dynamics and microvascular dilation under resting-state conditions and
during functional hyperemia in awake AD and WT mice. The same imaging fields of view were imaged on
days 0, 7, and 14 of the LPS challenge.

Fig. 2A displays example measurements of resting-state, spontaneous Ca2+ release from astrocytic
compartments over the course of the 14-day inflammatory challenge. Similar to pre-LPS resting state
measurements, raster scanning was performed in $\sim$100 μm^2 cortical regions surrounding penetrating arterioles
for 10 min at $\sim$ 4.4 Hz. We observed no discernible differences in cell morphology from days 0 – 14. Dynamic
Ca2+ transients were quantified and analyzed from the soma, processes, and endfoot compartments of
astrocytes (Figs 2 B &C). During the 14 day period, we observed variations in spontaneous Ca2+ fluctuations
in astrocytes in both cohorts, with some cell compartments demonstrating no Ca2+ transients over the 10 minute
measurement. Fig 2.D illustrates how the proportion of these 'silent,' quiescent cell compartments changed
during the inflammatory period. Among the cells that remained active in both AD and WT cohorts, the
frequency of spontaneous Ca2+ spikes progressively lowered during the 14-day period within astrocyte soma
and process compartments (figs 2 E&G).

Figure 2. LPS induced inflammation decreased spontaneous Ca2+ release in astrocytes in AD mice cortex. (A)
Raster scan image of cortical vasculature and astrocytes at different days during 14-days of LPS-induced systemic
inflammation. (B) Spontaneous Ca^{2+} release form astrocyte compartments in WT and AD mice cortex measured on pre-
LPS injection (day 0), after 7 and 14 days of LPS injection (day 7 and day14). (D) Variations in spontaneous Ca2+ activity
from astrocyte compartments during the 14-day period. (E-G) Quantification of astrocyte Ca2+ spikes under the impact
of LPS induced inflammation. Linear mixed effect model was used to test the effect of LPS injection.

To determine whether prolonged systemic inflammation impacts astrocytic contributions to functional
hyperemia, we examined arteriolar dilation and astrocyte Ca^+ release in response to brief (3s) and sustained
(30 s) pneumatic whisker stimulation. For short 3s whisker stimulation, arteriole dilation responses did not
change appreciably during the 14-day period for both AD and WT mice (figs 3 A & E), while astrocyte Ca2+
responses varied significantly. In the astrocyte soma of WT mice, Ca2+ release parameters showed reductions
in peak response and AUC between days 0 and 7 (fig 3.B, p-val = 0.036 and p-val = 0.047, respectively). For
both AD and WT mice, systemic inflammation substantially altered Ca2+ release in astrocyte processes,
provoking significant reductions in peak Ca2+ release, AUC, and rise time (figs 3D and 3H), and peak latency
in WT mice (supplementary figure 2). Interestingly, the inflammatory threat induced opposing effects in AD
and WT mice within astrocyte endfeet. In WT mice, we observed significant increases in peak Ca2+ of endfeet
and shorter response duration. Conversely, in AD mice, endfeet showed reduced peak Ca2+ and significantly
longer rise times, but longer duration (figs 3 C&G, supplementary figure 2).

Figure 3. Effect of LPS induced inflammation on penetrating arterial dilation and astrocyte Ca²⁺ release in response to brief whisker 3s stimulation. **(A&E)** Trial-averaged profiles and calculated features of stimulus-induced penetrating arteriole dilation and astrocyte Ca²⁺ release in WT and AD mice on day 0, day7 and day14 of LPS injection. **B-H** Trial-averaged profiles and calculated features of stimulus-induced, compartment-specific astrocyte Ca²⁺ release in WT and AD mice on day 0, day7 and day14 of LPS injection.

For sustained trials with longer 30 second whisker stimulation, the 14-day inflammatory threat provoked more pronounced alterations to WT mice than AD mice. Additionally, more significant alterations were observed in astrocytes than arterioles. In both AD and WT mice, inflammation provoked notable, yet not significant, reductions in arteriole dilation at days 7 and 14. Following stimulus cessation, arterioles returned to their baseline value significantly faster in AD mice, evidenced by the significantly reduced fall time (Supplementary figure 2). In WT mice, peak Ca2+ release, rise times, and peak latency during the entire 30 s stimulation all significantly decreased in soma and processes over the course of the 14 day inflammatory period, and AUC significantly lowered within all compartments. Maximum Ca2+ release during the late phase of stimulation were also significantly reduced in all compartments (fig4 a-d). In AD mice, the inflammatory threat provoked significant reductions in peak Ca2+ release from all astrocyte compartments. The AUC for responses in astrocyte endfeet also decreased significantly during the 14 day period in AD mice, while astrocyte processes showed significant reductions in AUC, peak latency, duration, and maximal fluorescence during the later plateau phase (fig 4 H and supplementary figure 3). Overall, our observations of reduced endfeet Ca2+ release correlate with mildly reduced p.a. dilation at the late phase of stimulation aligns well with prior studies

demonstrating that astrocyte Ca2+ help sustain arteriole dilation in response to prolonged functional
stimulation [26].

Capillaries also regulate cerebral blood flow through pericyte- and astrocyte-mediated dilation [27]. Systemic
inflammation increases neutrophils in brain capillaries, causing capillary stalling, and impairs cerebral blood
flow [11]. Using rapid line scan measurements, we measured kinetic profiles of stimulus induced vessel
dilation in higher order arterioles and capillary branches. Baseline vessel diameters were computed as the mean
diameter during the initial 5s prior to whisker stimulation. In WT mice, we observed a significant reduction in
baseline capillary diameters for 3rd order capillaries at days 7 and 14 of LPS-induced inflammation
(supplementary figure 4).

We then examined how inflammation impacts capillary dilation in response to functional stimulation. Trial-
averaged line scan measurements indicate that LPS injection yielded smaller capillary responses to sustained
stimulation (Supplementary Figure 4); however, we observed few statistically significant changes.

We also calculated RBC velocity in high-order (> 3rd-order) capillaries (supplementary figure 4). In WT mice,
3s stimulus-evoked RBC velocity (RBCv) change was lower on day 7 relative to baseline. While in AD mice,
RBCv was decreased on day 7 but increased on day 14 compared to day 0. Our data further support our
observations for vessel dilation in high-order capillaries. Both raster and line scan measurement of capillary
dilation and RBC velocity demonstrated that AD mice respond to LPS-induced inflammation differently than
WT, with LPS reduced capillary response in WT mice while increase capillary response in AD mice brain.

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Figure 4. Effect of LPS induced inflammation on cerebral vessel dilation and astrocyte Ca^{2+} release in response to sustained whisker stimulation. (A-D) Two-photon raster scanning measurement of 30s whisker stimulation induced penetrating arteriole dilation and astrocyte Ca^{2+} release in WT mice measured on day 0, day 7 and day 14 of LPS injection.

3.5 Ex vivo immunofluorescence analysis of LPS-induced inflammation and $A\beta_{1-42}$ accumulation

To assess neuroinflammation induced after 14 days of LPS injection, we harvested brains from subgroups of mice from each cohort for immunofluorescence (IF) staining of GFAP, Iba-1, and Aβ1-42 (n = 3 per cohort). We also analyzed a sham group of mice that received 14 days of saline injections (n=3 for AD, n=2 for WT). Fig. 5A displays representative confocal images of immunofluorescence staining. We quantified GFAP expression in astrocytes and IBA1 expression in microglia by calculating the percentage area of GFAP and IBA1 expressed cells in the confocal images (Fig. 5B). In saline control group, AD mice showed significantly increased GFAP expression in both cortex and hippocampus compared to WT mice, indicating a pre-existing neuroinflammation in AD mice brain. IBA-1 expression is slightly, but not significantly, higher than in AD control compared to WT control mice. After 7 days of LPS injection, GFAP and IBA1 expression in the WT brain both increased, with a statistically significant increase observed in GFAP expression. Interestingly, GFAP expression in AD astrocytes decreased after 7 days of LPS injection while microglial expression of IBA1 increased, suggesting AD astrocytes react to LPS-induced inflammation differently compared to WT animal. Both GFAP and IBA1 expression reduced after 14 days of LPS injection in both cohorts. This trend of recovery agrees well with our previous study exploring cortical oxygen extraction during 14 days of LPS injection [28]. The results could

reflect immune tolerance induced by the repeated injection of low-dose LPS [29–31]. Fig. 5C shows the
representative widefield fluorescence imaging of Aβ$_{1-42}$ in the cortex and hippocampus of AD mice. Strikingly,
14 days of LPS injection yielded reduced $A\beta_{1-42}$ load in AD mice brain, showing statistical significance in
cortex and a strong trend in the hippocampus (Fig. 5D). LPS injection induced $A\beta_{1-42}$ reduction was also
reported by other studies [32–34]. Higher $A\beta_{1-42}$ load was observed in the cortex compared to hippocampus
(Fig. 5D), agreeing well with previous reports in APPswe/PS1dE9 mice [35,36].

Figure 5. *Ex vivo* immunofluorescence imaging. (A) Immunofluorescence image of $A\beta_{1-42}$ In AD mice received 14 days
of saline injection (n=3), 7 days of LPS injection (n=2) and 14 days of LPS injection (n=3). (B) Quantification of Aβ$_{1-42}$
in cerebral cortex and hippocampus. Aβ$_{1-42}$ load was quantified using the percentage area. Multiple ROIs were quantified
and averaged for each animal. Data shown as the mean $\pm$ sem.(C) Representative confocal immunofluorescence image of
GFAP and Iba-1expression in barrel cortex and hippocampus in WT and AD mice. Images were taken under a 10X
objective. Scale bar = 100 μm. (D) Percentage area of GFAP and IBA-1 expression in barrel cortex and hippocampus.
One-way ANOVA with Tukey's post hoc test was used in (B) and (D) to test the difference between saline, 7 days LPS
and 14 days LPS injection. Differences between WT and AD saline control group in (B) and (D) were tested using
Student's t test. *p<0.05, **p<0.01, ***p<0.001.
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4. DISCUSSION

Astrocytes perform multifactorial functions for regulating both cerebral energetics and neuroimmunity. We hypothesized that Amyloid deposition in 12-13 month old APP/Swe mice provokes inflammatory alterations that yield disruptions to the mechanisms by which astrocyte Ca2+ modulates cerebral blood flow on both penetrating arterioles and capillaries. We posited that a pronounced systemic inflammatory threat would further exacerbate astrocyte contributions to resting state CBF and functional hyperemia.

Under resting state conditions, in the absence of an inflammatory threat, our observations revealed that 12- to 13-month-old female APPswe/PS1dE9 mice exhibit increased spontaneous astrocyte Ca^{2+} release and decreased astrocyte Ca^{2+} response to sustained 30s whisker stimulation compared to WT control mice (Figs. 1–3). 14 days of systemic inflammation suppresses both spontaneous and sensory stimulation-evoked astrocyte Ca^{2+} release in the barrel cortex of WT and AD mice and induced moderate changes to vascular response in arterioles and capillaries. Interestingly, LPS treatment also reduced $A\beta_{1-42}$ levels in the cortex and hippocampus of AD mice.

4.1 Astrocyte Ca^{2+} signaling in AD

Reactive astrocytes with elevated spontaneous Ca^{2+} release had been found in AD mice brains, especially near amyloid plaques [37,38]. Indeed, astrocytes were activated in our 12-month-old APP/P1dE9 mice brain, as indicated by increased GFAP expression in cortex and hippocampus compared with WT mice (Fig. 5) and exhibited increased frequency of spontaneous Ca^{2+} events of cortical astrocytes (Fig. 1). The exact mechanism of aberrant Ca^{2+} in reactive astrocyte is not fully understood. Upregulation of the purinergic and the metabotropic receptors and increased mitochondria Ca^{2+} efflux could explain the increased Ca^{2+} activity in reactive astrocytes [9]. While many studies explored the mechanisms underpinning astrocyte hyperactivity at the resting state, few studies have explored reactive astrocyte Ca^{2+} signaling during functional brain activation [39]. Our observation of reduced astrocyte Ca^{2+} release in AD mice in response to 30s whisker stimulation support prior findings of astrocyte Ca^{2+} activity under sensory-evoked stimulation (Fig. 2, 3). Lines et al also reported increased spontaneous release of Ca^{2+} and decreased hind-paw stimulation evoked responses in astrocytes in 6-month APP/PS1 mice [39]. Interestingly, a study revealed a negative correlation between the amplitude (i.e., absolute change) of the evoked Ca2+ signal and its baseline level [40]. In our AD mice, the declined astrocyte Ca^{2+} response was substantially more pronounced in response to 30s whisker stimulation compared to 3s of stimulation (Fig. 3, supplementary figure 2). The diminished Ca^{2+} release as stimulation persists could be attributed to insufficient Ca^{2+} storage in astrocytes. Lia et al. demonstrated astrocyte hypoactivity in response to ATP and noradrenaline (NA) in 6-month-old PS2APP mice and associated the

reduced Ca^{2+} level with reduced endoplasmic reticulum Ca^{2+} concentration [41]. Future studies measuring the

store concentration of Ca^{2+} in astrocytes could help to address our hypothesis [42].

Conflicting observations of astrocyte Ca^{2+} activity in AD mice model have been reported previously. Shah et

al. showed decreased calcium signaling in cingulate astrocytes in APP[NL-F] mice before the formation of amyloid

deposits [8]. The decreased astrocyte Ca^{2+} accounts for increased functional connectivity observed with

functional MRI. In 6-month-old PS2APP mice with the presence of Aβ deposit, Lia et al. found declined

spontaneous astrocyte cytosolic Ca^{2+} release, and the hypoactivity is independent with Aβ-plaque

proximity [41]. The findings regarding astrocyte activity in AD mice vary with the brain region, disease stage,

and animal model being studied. Interestingly, our results show mild reductions in vascular response to 3-

second and 30-second whisker stimulation in AD mice, indicating only modest differences in stimulus induced

blood volume changes between the 2 cohorts.

4. 2 Neurovascular coupling in AD brain

Impaired neurovascular coupling has been reported in AD patients and AD mouse models, including Tg2576,

J20 mouse and the triple transgenic 3xTg-AD mice [41,43–47]. Our OISI and in vivo imaging with two-photon

microscopy showed that 12-month-old female APP/PS1dE9 mice did not exhibit significant alterations in

cerebral vascular responses to whisker stimulation (Fig. 1, Supplementary Figure 1). However, dilation in high-

order capillaries (diameter < 5 μm) was significantly reduced in AD mice compared to WT (Supplementary fig.

1). The results indicate that disrupted neurovascular coupling originates within microvessels in the

APP/PS1dE9 mice. Preserved hemodynamic response in cortical arterioles was also reported in the familiar

AD mouse model J20 [48,49]. Gutiérrez-Jiménez et al. found reduced resting-state capillary flux and elevated

electrical stimulation evoked arteriole dilation and capillary RBC velocity in 18-month-old APPswe/PS1dE9

model compared with control mice group [50]. Conversely, early microvascular pathologies were detected in

APPswe/PS1dE9 mice with electron microscopy [51] and in 3x-Tg mice with optical coherence

tomography [52]. Taken together, our observations and these prior studies indicate that impairments to

neurovascular coupling in AD originates in micro vessels at early stages and then spreads to arterioles as the

disease progresses.

4.3 Neurovascular coupling in systemic inflammation

Previous studies demonstrated that LPS-induced systemic inflammation alters brain hemodynamic responses,

including increasing capillary stalling [11,53,54]. Here, we showed that 14 days of LPS-induced systemic

inflammation mildly reduced vascular dilation in response to brief 3 s whisker stimulation (Fig. 3,

supplementary figure 2), and more pronouncedly reduced hemodynamic response to sustained 30 whisker

stimulation in WT and AD mice (Fig. 4, supplementary figure 3). Prior studies focused on the acute effect of a single high-dose LPS injection (>1 mg/kg) and examined the cerebrovascular function within 24 hours after the injection [11,53]. In our study, we used a lower dose of LPS (0.3 mg/kg) and assessed its chronic effects by administering LPS continuously for 14 days and measuring vascular responses to whisker stimulation on days 7 and 14. Repeated, daily intraperitoneal injections (i.p.) of low-dose LPS (less than 1 mg/kg) in mice have been shown to induce immune tolerance at the later phases of the challenge. Several groups administrated 4 days of daily i.p. injections of low-dose LPS in C57BL/6J mice and 3-month-old APP23 mice [30,29,31]. They measured brain cytokine levels and found increased proinflammatory cytokines (e.g., IL-1β and TNF-α) during the first two days of injections, followed by significantly reduced cytokine levels starting on day 3, despite continued LPS exposure. Meanwhile, anti-inflammatory cytokines, such as IL-10 and TGF-β, increased during the later stages of treatment. These findings suggest a diminishing inflammatory response following the low-dose, repeated systemic administration of LPS. Similarly, our IF result showed unaltered GFAP and Iba-1 expression in astrocytes and microglia after 14 days of LPS injection (Fig. 5). Taken together, the diminished inflammatory response could explain why we did not observe detectable alterations in vascular response and glial activation under LPS injection. Additionally, LPS injection did not change the resting-state diameter of cortical penetrating and the precapillary arterioles in either mouse cohort. Only WT mice showed constriction in high-order capillaries after LPS administration (Fig. 4). Our recent study showed that 14 days of low-dose LPS administration did not affect resting state red blood cell flux in capillaries [28]. The reduced resting-state capillary diameter but preserved RBC flux might indicate a reduction in baseline capillary flow.

4.4 Systemic inflammation alters astrocyte Ca2+ signaling

While vascular responses appeared to be mildly reduced during prolonged inflammation, astrocyte Ca²⁺ levels were more heavily impacted. Astrocyte Ca²⁺ levels on day 14 showed no signs of recovery in either WT or AD mice and were further decreased in AD mice (Fig. 2). This persistent decline in astrocyte Ca²⁺ release, particularly in AD mice, suggests that other disruptions, such as impaired neuronal activity, may contribute to the observed deficits. Moreover, the reduction in astrocyte Ca²⁺ is linked with reduced $A\beta_{1-42}$ in AD mice cortex and hippocampus (Fig. 5). Many studies showed systemic LPS injection ameliorates amyloid pathology [33,55,32,34]. The involvement of astrocyte Ca²⁺ signaling in this process requires further investigation. Strikingly, in our APP/PS1dE9 mouse model, LPS substantially reduced sensory stimulation-evoked astrocyte Ca²⁺ while only mildly affecting arteriole dilation (Figs. 3 and 4). Instead, capillary dilation was decreased in AD mice (Fig. 4). The role of astrocyte Ca²⁺ in regulating cerebral blood flow during functional hyperemia remains uncertain and widely-debated [6]. Silencing astrocyte Ca²⁺ using CalEx affects arteriole dilation during sustained sensory stimulation, with no impact on brief sensory stimulation. Notably,

only the late phase of vessel dilation during sustained stimulation was reduced [26]. Other studies showed astrocyte Ca2+ signaling mediates neurovascular signaling to capillary pericytes but not arterioles [56]. LPS has been shown to cause pericyte loss and microvascular dysfunction [57,58]. Further studies investigating neurovascular coupling in capillary pericytes and astrocyte Ca^{2+} signaling under AD-related inflammation could offer greater insights.

Lastly, astrocyte Ca^{2+} also plays a pivotal role in regulating neuronal activity and synaptic plasticity [59]. LPS-induced systemic inflammation causes neuronal hyperexcitability [60,61]. Increased neuronal activity was also reported in the early stages of AD [62]. Our recent study showed that 14 days of systemic injection of LPS increased oxygen extraction in the somatosensory cortex in 8–to 9-month-old APP/PS1dE9 mice and the age-matched control [28]. Therefore, the reduced Ca^{2+} levels in astrocyte soma and processes under AD and LPS may be linked to alterations in neuronal activity during functional brain activation.

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References

1. V. Calsolaro and P. Edison, "Neuroinflammation in Alzheimer's disease: Current evidence and future directions," Alzheimer's & Dementia **12**, 719–732 (2016).

2. M. T. Heneka, M. J. Carson, J. E. Khoury, G. E. Landreth, F. Brosseron, D. L. Feinstein, A. H. Jacobs, T. Wyss-Coray, J. Vitorica, R. M. Ransohoff, K. Herrup, S. A. Frautschy, B. Finsen, G. C. Brown, A. Verkhratsky, K. Yamanaka, J. Koistinaho, E. Latz, A. Halle, G. C. Petzold, T. Town, D. Morgan, M. L. Shinohara, V. H. Perry, C. Holmes, N. G. Bazan, D. J. Brooks, S. Hunot, B. Joseph, N. Deigendesch, O. Garaschuk, E. Boddeke, C. A. Dinarello, J. C. Breitner, G. M. Cole, D. T. Golenbock, and M. P. Kummer, "Neuroinflammation in Alzheimer's disease," The Lancet Neurology **14**, 388–405 (2015).

3. C. Iadecola, "Neurovascular regulation in the normal brain and in Alzheimer's disease," Nat Rev Neurosci **5**, 347–360 (2004).

4. B. V. Zlokovic, "Neurovascular pathways to neurodegeneration in Alzheimer's disease and other disorders," Nat Rev Neurosci **12**, 723–738 (2011).

5. E. Colombo and C. Farina, "Astrocytes: Key Regulators of Neuroinflammation," Trends in Immunology **37**, 608–620 (2016).

6. A. Lia, A. Di Spiezio, M. Speggiorin, and M. Zonta, "Two decades of astrocytes in neurovascular coupling," Front. Netw. Physiol. **3**, 1162757 (2023).

7. G. R. Frost and Y.-M. Li, "The role of astrocytes in amyloid production and Alzheimer's disease," Open Biol. **7**, 170228 (2017).

8. D. Shah, W. Gsell, J. Wahis, E. S. Luckett, T. Jamoulle, B. Vermaercke, P. Preman, D. Moechars, V. Hendrickx, T. Jaspers, K. Craessaerts, K. Horré, L. Wolfs, M. Fiers, M. Holt, D. R. Thal, Z. Callaerts-Vegh, R. D'Hooge, R. Vandenberghe, U. Himmelreich, V. Bonin, and B. De Strooper, "Astrocyte calcium dysfunction causes early network hyperactivity in Alzheimer's disease," Cell Reports **40**, 111280 (2022).

9. E. Shigetomi, K. Saito, F. Sano, and S. Koizumi, "Aberrant Calcium Signals in Reactive Astrocytes: A Key Process in Neurological Disorders," Int J Mol Sci **20**, 996 (2019).

10. A. Verkhratsky, "Astroglial Calcium Signaling in Aging and Alzheimer's Disease," Cold Spring Harb Perspect Biol **11**, a035188 (2019).

11. S. K. Fruekilde, C. J. Bailey, K. L. Lambertsen, B. H. Clausen, J. Carlsen, N. Xu, K. R. Drasbek, and E. Gutiérrez-Jiménez, "Disturbed microcirculation and hyperaemic response in a murine model of systemic inflammation," J Cereb Blood Flow Metab 0271678X2211122 (2022).

12. L. E. Evans, J. L. Taylor, C. J. Smith, H. A. T. Pritchard, A. S. Greenstein, and S. M. Allan, "Cardiovascular comorbidities, inflammation, and cerebral small vessel disease," Cardiovascular Research cvab284 (2021).

13. S. B. Sankar, A. F. Pybus, A. Liew, B. Sanders, K. J. Shah, L. B. Wood, and E. M. Buckley, "Low cerebral blood flow is a non-invasive biomarker of neuroinflammation after repetitive mild traumatic brain injury," Neurobiol Dis **124**, 544–554 (2019).

14. C. R. A. Batista, G. F. Gomes, E. Candelario-Jalil, B. L. Fiebich, and A. C. P. de Oliveira, "Lipopolysaccharide-Induced Neuroinflammation as a Bridge to Understand Neurodegeneration," IJMS **20**, 2293 (2019).

15. L. Qin, X. Wu, M. L. Block, Y. Liu, G. R. Breese, J.-S. Hong, D. J. Knapp, and F. T. Crews, "Systemic LPS causes chronic neuroinflammation and progressive neurodegeneration," Glia **55**, 453–462 (2007).

16. J. L. Jankowsky, D. J. Fadale, J. Anderson, G. M. Xu, V. Gonzales, N. A. Jenkins, N. G. Copeland, M. K. Lee, L. H. Younkin, S. L. Wagner, S. G. Younkin, and D. R. Borchelt, "Mutant presenilins specifically elevate the levels of the 42 residue β-amyloid peptide in vivo: evidence for augmentation of a 42-specific γ secretase," Human Molecular Genetics **13**, 159–170 (2004).

17. K. Kılıç, M. Desjardins, J. Tang, M. Thunemann, S. Sunil, Ş. E. Erdener, D. D. Postnov, D. A. Boas, and A. Devor, "Chronic Cranial Windows for Long Term Multimodal Neurovascular Imaging in Mice," Front. Physiol. **11**, 612678 (2021).

18. R. L. Lowery and A. K. Majewska, "Intracranial Injection of Adeno-associated Viral Vectors," JoVE 2140 (2010).

19. A. Y. Shih, J. D. Driscoll, P. J. Drew, N. Nishimura, C. B. Schaffer, and D. Kleinfeld, "Two-Photon Microscopy as a Tool to Study Blood Flow and Neurovascular Coupling in the Rodent Brain," J Cereb Blood Flow Metab **32**, 1277–1309 (2012).

20. E. A. Pnevmatikakis and A. Giovannucci, "NoRMCorre: An online algorithm for piecewise rigid motion correction of calcium imaging data," Journal of Neuroscience Methods **291**, 83–94 (2017).

21. R. Srinivasan, B. S. Huang, S. Venugopal, A. D. Johnston, H. Chai, H. Zeng, P. Golshani, and B. S. Khakh, "Ca2+ signaling in astrocytes from Ip3r2−/− mice in brain slices and during startle responses in vivo," Nat Neurosci **18**, 708–717 (2015).

22. J. L. Stobart, K. D. Ferrari, M. J. P. Barrett, M. J. Stobart, Z. J. Looser, A. S. Saab, and B. Weber, "Long-term In Vivo Calcium Imaging of Astrocytes Reveals Distinct Cellular Compartment Responses to Sensory Stimulation," Cerebral Cortex **28**, 184–198 (2018).

23. J. N. Haidey, G. Peringod, A. Institoris, K. A. Gorzo, W. Nicola, M. Vandal, K. Ito, S. Liu, C. Fielding, F. Visser, M. D. Nguyen, and G. R. Gordon, "Astrocytes regulate ultra-slow arteriole oscillations via stretch-mediated TRPV4-COX-1 feedback," Cell Reports **36**, 109405 (2021).

24. M. J. P. Barrett, K. D. Ferrari, J. L. Stobart, M. Holub, and B. Weber, "CHIPS: an Extensible Toolbox for Cellular and Hemodynamic Two-Photon Image Analysis," Neuroinform **16**, 145–147 (2018).

25. P. Y. Chhatbar and P. Kara, "Improved blood velocity measurements with a hybrid image filtering and iterative Radon transform algorithm," Front. Neurosci. **7**, (2013).

26. A. Institoris, M. Vandal, G. Peringod, C. Catalano, C. H. Tran, X. Yu, F. Visser, C. Breiteneder, L. Molina, B. S. Khakh, M. D. Nguyen, R. J. Thompson, and G. R. Gordon, "Astrocytes amplify neurovascular coupling to sustained activation of neocortex in awake mice," Nat Commun **13**, 7872 (2022).

27. S. Grubb, M. Lauritzen, and C. Aalkjær, "Brain capillary pericytes and neurovascular coupling," Comparative Biochemistry and Physiology Part A: Molecular & Integrative Physiology **254**, 110893 (2021).

28. C. Liu, A. Cárdenas-Rivera, S. Teitelbaum, A. Birmingham, M. Alfadhel, and M. A. Yaseen, "Neuroinflammation
increases oxygen extraction in a mouse model of Alzheimer's disease," Alz Res Therapy **16**, 78 (2024).

29. J. Kim, O. Sullivan, K. Lee, J. Jao, J. Tamayo, A. M. Madany, B. Wong, P. Ashwood, and A. V. Ciernia, "Repeated
LPS induces training and tolerance of microglial responses across brain regions," J Neuroinflammation **21**, 233
(2024).

30. A.-C. Wendeln, K. Degenhardt, L. Kaurani, M. Gertig, T. Ulas, G. Jain, J. Wagner, L. M. Häsler, K. Wild, A.
Skodras, T. Blank, O. Staszewski, M. Datta, T. P. Centeno, V. Capece, Md. R. Islam, C. Kerimoglu, M.
Staufenbiel, J. L. Schultze, M. Beyer, M. Prinz, M. Jucker, A. Fischer, and J. J. Neher, "Innate immune memory in
the brain shapes neurological disease hallmarks," Nature **556**, 332–338 (2018).

31. D. M. Norden, P. J. Trojanowski, E. Villanueva, E. Navarro, and J. P. Godbout, "Sequential activation of microglia
and astrocyte cytokine expression precedes increased iba‐1 or GFAP immunoreactivity following systemic
immune challenge," Glia **64**, 300–316 (2016).

32. C. Thygesen, L. Ilkjær, S. J. Kempf, A. L. Hemdrup, C. U. von Linstow, A. A. Babcock, S. Darvesh, M. R. Larsen,
and B. Finsen, "Diverse Protein Profiles in CNS Myeloid Cells and CNS Tissue From Lipopolysaccharide- and
Vehicle-Injected APPSWE/PS1ΔE9 Transgenic Mice Implicate Cathepsin Z in Alzheimer's Disease," Front. Cell.
Neurosci. **12**, 397 (2018).

33. T. M. Malm, M. Koistinaho, M. Pärepalo, T. Vatanen, A. Ooka, S. Karlsson, and J. Koistinaho, "Bone-marrow-
derived cells contribute to the recruitment of microglial cells in response to β-amyloid deposition in APP/PS1
double transgenic Alzheimer mice," Neurobiology of Disease **18**, 134–142 (2005).

34. C. Jendresen, A. Digre, H. Cui, X. Zhang, I. Vlodavsky, J.-P. Li, and L. N. G. Nilsson, "Systemic LPS-induced Aβ-
solubilization and clearance in AβPP-transgenic mice is diminished by heparanase overexpression," Sci Rep **9**,
4600 (2019).

35. C. U. Von Linstow, J. Waider, M. Grebing, A. Metaxas, K. P. Lesch, and B. Finsen, "Serotonin augmentation
therapy by escitalopram has minimal effects on amyloid-β levels in early-stage Alzheimer's-like disease in mice,"
Alz Res Therapy **9**, 74 (2017).

36. A. Willuweit, M. Schöneck, S. Schemmert, P. Lohmann, S. Bremen, D. Honold, N. Burda, N. Jiang, S. Beer, J.
Ermert, D. Willbold, N. J. Shah, and K.-J. Langen, "Comparison of the Amyloid Load in the Brains of Two
Transgenic Alzheimer's Disease Mouse Models Quantified by Florbetaben Positron Emission Tomography,"
Front. Neurosci. **15**, 699926 (2021).

37. K. V. Kuchibhotla, C. R. Lattarulo, B. T. Hyman, and B. J. Bacskai, "Synchronous Hyperactivity and Intercellular
Calcium Waves in Astrocytes in Alzheimer Mice," Science **323**, 1211–1215 (2009).

38. A. Delekate, M. Füchtemeier, T. Schumacher, C. Ulbrich, M. Foddis, and G. C. Petzold, "Metabotropic P2Y1
receptor signalling mediates astrocytic hyperactivity in vivo in an Alzheimer's disease mouse model," Nat
Commun **5**, 5422 (2014).

39. J. Lines, A. M. Baraibar, C. Fang, E. D. Martin, J. Aguilar, M. K. Lee, A. Araque, and P. Kofuji, "Astrocyte‐
neuronal network interplay is disrupted in Alzheimer's disease mice," Glia **70**, 368–378 (2022).

40. C. M. King, K. Bohmbach, D. Minge, A. Delekate, K. Zheng, J. Reynolds, C. Rakers, A. Zeug, G. C. Petzold, D. A.
Rusakov, and C. Henneberger, "Local Resting Ca2+ Controls the Scale of Astroglial Ca2+ Signals," Cell Reports
30, 3466-3477.e4 (2020).

41. A. Lia, G. Sansevero, A. Chiavegato, M. Sbrissa, D. Pendin, L. Mariotti, T. Pozzan, N. Berardi, G. Carmignoto, C.
Fasolato, and M. Zonta, "Rescue of astrocyte activity by the calcium sensor STIM1 restores long-term synaptic
plasticity in female mice modelling Alzheimer's disease," Nat Commun **14**, 1590 (2023).

42. J. Suzuki, K. Kanemaru, K. Ishii, M. Ohkura, Y. Okubo, and M. Iino, "Imaging intraorganellar Ca2+ at subcellular
resolution using CEPIA," Nat Commun **5**, 4153 (2014).

43. Y. Iturria-Medina, R. C. Sotero, P. J. Toussaint, J. M. Mateos-Pérez, A. C. Evans, and Alzheimer's Disease
Neuroimaging Initiative, "Early role of vascular dysregulation on late-onset Alzheimer's disease based on
multifactorial data-driven analysis," Nat Commun **7**, 11934–11934 (2016).

44. S. Tarantini, C. H. T. Tran, G. R. Gordon, Z. Ungvari, and A. Csiszar, "Impaired neurovascular coupling in aging
and Alzheimer's disease: Contribution of astrocyte dysfunction and endothelial impairment to cognitive decline,"
Experimental Gerontology **94**, 52–58 (2017).

45. L. Park, J. Zhou, K. Koizumi, G. Wang, A. Anfray, S. J. Ahn, J. Seo, P. Zhou, L. Zhao, S. Paul, J. Anrather, and C.
Iadecola, "tPA Deficiency Underlies Neurovascular Coupling Dysfunction by Amyloid-β," J. Neurosci. **40**, 8160–
8173 (2020).

46. L. Li, X.-K. Tong, M. Hosseini Kahnouei, D. Vallerand, E. Hamel, and H. Girouard, "Impaired Hippocampal
Neurovascular Coupling in a Mouse Model of Alzheimer's Disease," Front. Physiol. **12**, 715446 (2021).

47. C. F. Lourenço, A. Ledo, R. M. Barbosa, and J. Laranjinha, "Neurovascular uncoupling in the triple transgenic
model of Alzheimer's disease: Impaired cerebral blood flow response to neuronal-derived nitric oxide signaling,"
Experimental Neurology **291**, 36–43 (2017).

48. P. S. Sharp, K. E. Ameen-Ali, L. Boorman, S. Harris, S. Wharton, C. Howarth, O. Shabir, P. Redgrave, and J.
Berwick, "Neurovascular coupling preserved in a chronic mouse model of Alzheimer's disease: Methodology is
critical," J Cereb Blood Flow Metab **40**, 2289–2303 (2020).

49. O. Shabir, B. Pendry, L. Lee, B. Eyre, P. S. Sharp, M. A. Rebollar, D. Drew, C. Howarth, P. R. Heath, S. B.
Wharton, S. E. Francis, and J. Berwick, "Assessment of neurovascular coupling and cortical spreading depression
in mixed mouse models of atherosclerosis and Alzheimer's disease," eLife **11**, e68242 (2022).

50. E. Gutiérrez-Jiménez, H. Angleys, P. M. Rasmussen, M. J. West, L. Catalini, N. K. Iversen, M. S. Jensen, S.
Frische, and L. Østergaard, "Disturbances in the control of capillary flow in an aged APPswe/PS1ΔE9 model of
Alzheimer's disease," Neurobiology of Aging **62**, 82–94 (2018).

51. P. Kelly, P. Denver, S. C. Satchell, M. Ackermann, M. A. Konerding, and C. A. Mitchell, "Microvascular
ultrastructural changes precede cognitive impairment in the murine APPswe/PS1dE9 model of Alzheimer's
disease," Angiogenesis **20**, 567–580 (2017).

52. K. W. Walek, S. Stefan, J.-H. Lee, P. Puttigampala, A. H. Kim, S. W. Park, P. J. Marchand, F. Lesage, T. Liu, Y.-
W. A. Huang, D. A. Boas, C. Moore, and J. Lee, "Near-lifespan longitudinal tracking of brain microvascular
morphology, topology, and flow in male mice," Nat Commun **14**, 2982 (2023).

53. G. Brezzo, J. Simpson, K. E. Ameen-Ali, J. Berwick, and C. Martin, "Acute effects of systemic inflammation upon
the neuro-glial-vascular unit and cerebrovascular function," Brain, Behavior, & Immunity - Health **5**, 100074
(2020).

54. B. Rosengarten, S. Wolff, S. Klatt, and R. T. Schermuly, "Effects of inducible nitric oxide synthase inhibition or
norepinephrine on the neurovascular coupling in an endotoxic rat shock model," Crit Care **13**, R139 (2009).

55. M. Go, J. Kou, J.-E. Lim, J. Yang, and K. Fukuchi, "Microglial response to LPS increases in wild-type mice during
aging but diminishes in an Alzheimer's mouse model: Implication of TLR4 signaling in disease progression,"
Biochemical and Biophysical Research Communications **479**, 331–337 (2016).

56. A. Mishra, J. P. Reynolds, Y. Chen, A. V. Gourine, D. A. Rusakov, and D. Attwell, "Astrocytes mediate
neurovascular signaling to capillary pericytes but not to arterioles," Nat Neurosci **19**, 1619–1627 (2016).

57. H. Zeng, X. He, Q. Tuo, D. Liao, G. Zhang, and J. Chen, "LPS causes pericyte loss and microvascular dysfunction
via disruption of Sirt3/angiopoietins/Tie-2 and HIF-2α/Notch3 pathways," Sci Rep **6**, 20931 (2016).

58. T. P. Carvalho, F. A. O. Toledo, D. F. A. Bautista, M. F. Silva, J. B. S. Oliveira, P. A. Lima, F. B. Costa, N. Q.
Ribeiro, J.-Y. Lee, A. Birbrair, T. A. Paixão, R. M. Tsolis, and R. L. Santos, "Pericytes modulate endothelial
inflammatory response during bacterial infection," mBio **15**, e03252-23 (2024).

59. N. Bazargani and D. Attwell, "Astrocyte calcium signaling: the third wave," Nat Neurosci **19**, 182–189 (2016).

60. R. Doenlen, U. Krügel, T. Wirth, C. Riether, A. Engler, G. Prager, H. Engler, M. Schedlowski, and G. Pacheco-
López, "Electrical activity in rat cortico-limbic structures after single or repeated administration of
lipopolysaccharide or staphylococcal enterotoxin B," Proc. R. Soc. B. **278**, 1864–1872 (2011).

61. K. Odoj, B. Brawek, N. Asavapanumas, N. Mojtahedi, M. T. Heneka, and O. Garaschuk, "In vivo mechanisms of
cortical network dysfunction induced by systemic inflammation," Brain, Behavior, and Immunity **96**, 113–126
(2021).

62. H. Targa Dias Anastacio, N. Matosin, and L. Ooi, "Neuronal hyperexcitability in Alzheimer's disease: what are the
drivers behind this aberrant phenotype?," Transl Psychiatry **12**, 257 (2022).