Effects of Nanopore Confinement on the Conformational, Dynamical, and Self-Assembly Properties of an FG-Repeat Peptide

Wancheng Zhao, Wai-Ming Yau, and Robert Tycko
Laboratory of Chemical Physics
National Institute of Diabetes and Digestive and Kidney Diseases
National Institutes of Health
Bethesda, MD 20892-0520

corresponding author: Dr. Robert Tycko, National Institutes of Health, Building 5, Room 409, Bethesda, MD 20892-0520; email robertty@mail.nih.gov; phone 301-402-8272

ABSTRACT

The central channels of nuclear pore complexes (NPCs) in eukaryotic cells contain a high concentration of protein chains with characteristic phenylalanine-glycine motifs, called FG-repeat domains, tethered to the channel walls. Passage of macromolecules and macromolecular assemblies between the cell nucleus and the cytoplasm depends on the dynamics of the FG-repeat domains and their interactions with nuclear transport receptors. Yet FG-repeat domains are highly aggregation-prone in free solution, forming amyloid-like fibrils at relatively low concentrations. Here we describe an approach to studying the properties of FG-repeat domains (or other polypeptides) when tethered to the walls of pores with diameters similar to those of NPC channels. By attaching alkyl phosphonate groups to the N-termini of 30-residue FG30 peptides that contain four FG repeats, we tether FG30 chains to walls of 20-nm-diameter pores in anodic aluminum oxide (AAO) wafers through phosphonate-surface bonds. Quantitative ^{13}C and ^{31}P nuclear magnetic resonance (NMR) measurements indicate 90 mM peptide concentrations (300 mg/ml) within the pores. One- and two-dimensional NMR spectra and nuclear spin relaxation measurements show that FG30 chains are dynamically disordered and random-coil-like in buffer-filled pores over a broad temperature range, with no sign of aggregation over many weeks despite the high intrapore concentrations. In contrast, the same FG30 peptide aggregates in free solution at 24° C at concentrations above 2 mM, forming structurally ordered fibrils according to electron microscopy and NMR measurements. These results demonstrate the utility of AAO as a scaffold for studying the properties of FG-repeat domains under conditions that mimic those within NPC channels, show that NMR measurements can elucidate these properties, and suggest that tethering to nanopore walls dramatically alters the self-assembly properties of FG-repeat domains, with potentially important implications for NPC function.

INTRODUCTION

The behavior of polypeptide chains when tethered to the inner surfaces of pores with diameters in the 10-100 nm range is biologically important in the context of the nuclear pore complexes (NPCs) of eukaryotic cells, which restrict and control the passage of proteins, RNA, and macromolecular complexes between the nucleus and the cytoplasm[1-3]. An NPC contains about 34 unique nuclear pore proteins (Nups) that form an intricate, eight-fold symmetric structure comprising outer and inner rings, a nuclear basket, and cytoplasmic filaments[4-5]. The central channel of a NPC, through which macromolecules and other chemical compounds must pass, has a diameter in the 40-80 nm range, depending on the organism and the state of the cell[4, 6-8].

Protein segments known as "FG-repeat domains", due to the presence of multiple phenylalanine-glycine pairs spaced 10-15 residues apart in their amino acid sequences, project into the central channel. FG-repeat domains are found at the N-terminal or C-terminal ends of Nups that participate in the NPC inner ring and vary in length from 150 to over 300 residues[5]. FG-repeat domains are examples of "low-complexity" (LC) sequences, in that they are relatively rich in glycine residues and residues with polar sidechains, contain relatively few residues with large hydrophobic sidechains, and contain few residues with charged sidechains[9]. FG-repeat domains are intrinsically disordered as monomers[10-14], as is true for other LC sequences[15-16]. FG-repeat domains are also known to be aggregation-prone, forming amyloid-like fibrils[11, 17-20] in analogy to the fibril-forming properties of other LC sequences[21-23].

The density of FG-repeat domains within the central channel is approximately 100-200 mg/ml[24], similar to the typical protein density in a liquid-liquid phase-separated protein "droplet"[15, 25]. The high density of FG-repeat domains within the central channel is believed to account for the ability of NPCs to impede uncontrolled diffusion of macromolecules and complexes with molecular weights greater than roughly 60 kDa through the central channel[26], with diffusion of smaller entities remaining relatively rapid due to the space between and flexibility of the FG-repeat domains. Rapid passage of large macromolecules and complexes through the NPC depends on binding to nuclear transport receptors (NTRs), which then interact transiently with FG motifs in a way that facilitates diffusion of an NTR/macromolecule complex through the densely filled channel[27-29].

Molecular details of the mechanism by which interactions between NTRs and FG-repeat domains facilitate diffusion through the central channel of an NPC are not fully understood[10, 28, 30]. To investigate this mechanism outside of biological cells and elucidate the properties of FG-repeat sequences at high concentrations, several approaches to creating partial mimics of NPC channels have been explored[31]. One approach is to form hydrogel particles from FG-repeat sequences[32-33]. While such hydrogel particles have been shown to exhibit size and sequence selectivity and NTR dependence similar to that of true NPC channels[32-34], they are considerably larger than and lack the pore geometry of an NPC. NTR dependence was also reported for liquid-like droplets formed by an FG-repeat sequence in a microfluidic system[35]. Another approach is to construct NPC-like pores, containing internally tethered FG-repeat sequences, with DNA origami methods[36-38]. While this approach allows precise control of dimensions, geometry, and FG-repeat density, DNA origami-based NPC mimics have been prepared only in small quantities, limiting the range of measurement techniques that can be applied. A third approach is to fabricate solid-state nanopores to which FG-repeat sequences can be attached[24, 39-41]. While this approach permits single-channel measurements of conductivity and transport, other types of measurements are precluded.

In principle, nuclear magnetic resonance (NMR) measurements can provide a wealth of

information about the conformational distributions, molecular motions, and self-assembly properties of FG-repeat domains, as well as effects of post-translational modifications, variations in solvent conditions, and interactions with NTRs on these properties. Several NMR studies of FG-repeat domains have been reported, providing information about residue-specific conformational preferences of the monomeric state[11, 13-14], interactions with NTRs in solution[13-14], molecular motions in hydrogel particles[12], and the nature of intermolecular interactions in FG-repeat hydrogels[20, 33].

NMR measurements on FG-repeat sequences that are tethered to nanopore walls at high concentrations would be particularly interesting, since such measurements would relate more directly to the properties of NPC channels. In particular, the fibril-forming propensity of isolated FG-repeat domains in free solution at concentrations well below the concentrations in NPC channels[11, 18] seems incompatible with the biological function of NPCs. NMR measurements in a nanopore environment could reveal whether such an environment affects FG-repeat aggregation, as well as other aspects of structure and dynamics. Unfortunately, quantities of FG-repeat sequences in previously developed nanopore mimics of NPCs, such as DNA origami constructs and solid-state nanopores, are grossly insufficient for NMR measurements.

This paper introduces a new method for creating samples in which FG-repeat sequences (or other polypeptides) are tethered to the walls of nanopores, with adequate quantities for detailed NMR studies. The method takes advantage of the reactivity of phosphonate groups with aluminum oxide surfaces[42-44] and the commercial availability of nanoporous anodic aluminum oxide (AAO) wafers that contain a high density of long pores with uniform diameters[45-46]. As depicted in Fig. 1, we report results from experiments on a 30-residue peptide from human Nup98, containing four FG motifs, which we call FG30. Nup98 was chosen due to its high density of FG motifs, its importance for NPC function, and its use in previous studies[11, 30, 33-34, 47-48]. We show that FG30 (and other peptides) can be tagged with an N-terminal phosphonate linker through cysteine-maleimide chemistry and covalently attached to surfaces within 20-nm-diameter AAO pores, achieving peptide concentrations within the pores up to 90 mM (300 mg/ml). NMR measurements reveal that the FG-repeat peptide remains highly flexible and dynamic in fully hydrated AAO pores over a wide temperature range, with no signs of aggregation over many weeks. In contrast, the same peptide aggregates to form fibrils in free solution at concentrations above 2 mM (7 mg/ml). Thus, aggregation of an FG-repeat sequence can be strongly inhibited by tethering to the walls of a nanopore. Our results establish the utility of AAO, phosphonate/aluminum oxide chemistry, and a variety of NMR measurements as an approach to studies of FG-repeat sequences in a nanopore environment that partially mimics the central channels of NPCs.

MATERIALS AND METHODS

Preparation of FG30 samples

C-FG30 peptides (sequence C-FGNNKLTTFGSSTTSAPSFGTTSGGLFGNK, with C-terminal amidation) were synthesized at a 0.1 mmol scale on a Biotage Initiator+ Alstra solid-phase peptide synthesizer, using standard Fmoc chemistry and activation with diisopropylcarbodiimide and OxymaPure in N-methyl-2-pyrrolidone. A rink amide ChemMatrix resin (Sigma-Aldrich) was used, with a substitution of 0.48 mEq/g as determined from the ultraviolet absorbance of the dibenzofulvene-piperidine adduct[49]. Peptides were synthesized with uniform ^{15}N,^{13}C-labeled residues at L6, S11, A16, F19, T22 and G28 (called C-FG30-LSAFTG)

or G2, G10, G20, and G29 (called C-FG30-4G). Unlabeled Fmoc-amino acids were coupled with a five-fold excess for 15 min at 75° C. Fmoc-Asn(Trt)-OH and Fmoc-Pro-OH were double-coupled, using 15 min at 75° C for each coupling. Isotopically labeled Fmoc-amino acids were coupled with a three-fold excess for 15 min at 75° C, followed by coupling of a five-fold excess of the corresponding unlabeled Fmoc-amino acids for 5 min at 75° C. Deprotection steps used 20% piperidine with 0.1M 1-Hydroxybenzotriazole hydrate in dimethyl formamide for 5 min at 75° C. Peptides were cleaved from the resin with a standard cocktail (8.75 ml trifluoroacetic acid, 0.75 g phenol, 0.5 ml thioanisole, 0.25 ml ethane-1,2-dithiol, 0.5 ml H_2O) for 2 h. After filtration and precipitation with cold t-butyl methyl ether (TBME), the crude product was further washed twice with TBME. Peptides were purified by reverse-phase high-performance liquid chromatography (HPLC) on a Proto 300 C18 column (Higgins Analytical).

To prepare 4-maleimidobutylphosphonic acid (MBPA), 4-aminobutylphosphonic acid (1 mmol, ChemScene) and maleic anhydride (1 mmol, Sigma-Aldrich) were suspended in 10 ml glacial acetic acid (Macron) and stirred overnight at room temperature. After the reaction was refluxed for an additional 5 h, n-heptane (25-30 ml, Alfa Aesar) was added to the reaction and glacial acetic acid was distilled off as an azeotrope. Addition of n-heptane and distillation were repeated three times. The desired product, 4-maleimidobutylphosphonic acid, was collected as an oil, dried under vacuum overnight, and used without further purification.

To conjugate MBPA to the N-terminal cysteine residue of C-FG30, C-FG30 (3 mmol) and MBPA (10 mmol) were dissolved in 2.0 ml of dimethyl formamide/water (1:1 by volume) and stirred at room temperature. Completion of the conjugation reaction that was monitored by liquid chromatography-mass spectrometry (LC-MS; Thermo Scientific UltiMate 3000 and ISQEM-ESI single quadrupole mass spectrometer). The final product was purified by HPLC on a Proto 300 C18 reverse-phase column (Higgins Analytical).

Melittin with an additional N-terminal cysteine (sequence C-GIGAVLKVLTTGLPALISWIKRKRQQ, with C-terminal amidation) and with uniform ^{15}N,^{13}C-labeled residues at G3, V8, and A15 was synthesized and purified with the same methods. MBPA was conjugated to the N-terminal cysteine to produce MBPA-C-melittin-GVA. Fig. S1 shows LC-MS results for MBPA-C-FG30-LSAFTG, MBPA-C-FG30-4G, and MBPA-C-melittin-GVA.

For confocal fluorescence imaging, MBPA-C-FG30 was labeled with fluorescein by reaction of fluorescein isothiocyanate (FITC) with the peptide amine groups. Approximately 2 mg of MBPA-C-FG30-4G was dissolved in 1 ml of sodium carbonate buffer (0.1 M, pH 9.0), and 1 mg of FITC was dissolved in anhydrous dimethyl sulfoxide (DMSO). The FITC solution was slowly added to the peptide solution in 50 µl aliquots, with gentle stirring. The reaction mixture was incubated in the dark at 4 °C for approximately 16 h. After confirming product formation by LC-MS, the reaction was quenched by addition of excess ammonium chloride, with a final concentration of 50 mM, and an additional incubation at 4 °C for 1 h. The final mixture was purified by preparative HPLC on the C18 reverse-phase column and subsequently lyophilized. LC-MS measurements indicated a single fluorescein per peptide molecule.

Aggregated MBPA-C-FG30 for transmission electron microscopy (TEM) was prepared by dissolving 2.0 mg of purified and lyophilized MBPA-C-FG30-LSAFTG in 60 µl of 0.2 M Bis-Tris buffer (pH 6.5) to produce a 10 mM peptide solution. The solution was evenly divided into three 20 µl aliquots, each transferred into a 0.2 ml tube. The three tubes were incubated quiescently for 6 days at temperatures of 4° C, 24° C, and 37° C. After incubation, each sample was briefly vortexed, and 3 µl was withdrawn for subsequent TEM imaging, as described below.

For NMR measurements on aggregated MBPA-C-FG30, a second 60 µl volume of 10 mM

MBPA-C-FG30-LSAFTG peptide solution was prepared in the same way, then incubated quiescently at 24° C for 13 days. Aggregated material was pelleted at 278,000 × g at 20° C for 120 min, using a Beckman Coulter Optima MAX ultracentrifuge with a TLA100.1 rotor. Approximately 3 mg of wet pellet, including residual buffer, was then transferred into a 3.2 mm magic-angle spinning (MAS) rotor by centrifugation at 71,000 × g and 4° C for 1 h using a Beckman Coulter Optima XL-100K Ultracentrifuge with an SW40Ti rotor. The aggregated sample remained fully hydrated throughout the subsequent NMR measurements.

NMR measurements

NMR measurements on MBPA-C-FG30 samples were performed at 14.1 T (599.1 MHz, 242.5 MHz, and 150.7 MHz frequencies for ^{1}H, ^{31}P, and ^{13}C, respectively) using a Tecmag Redstone spectrometer and a three-channel magic-angle spinning (MAS) NMR probe from Black Fox LLC. All measurements used MAS at 12.00 kHz. Sample temperatures were controlled with nitrogen gas from an FTS AirJet XR cooler. The dependence of sample temperature on nitrogen gas temperature and flow rate was determined from measurements on KBr powder[50] at 12.00 kHz MAS frequency in the same probe.

Additional NMR measurements on MBPA-C-melittin-GVA were performed at 17.5 T (744.6 MHz, 301.4 MHz, 187.2 MHz for ^{1}H, ^{31}P, and ^{13}C, respectively), also using a Tecmag Redstone spectrometer and a three-channel MAS NMR probe from Black Fox LLC, with MAS at 12.50 kHz. Sample temperatures were calibrated with measurements on KBr powder.

Radio-frequency (rf) pulse sequences for all NMR measurements on MBPA-C-FG30 are shown in Fig. S2, with information about pulse sequence parameters in the figure caption. One-dimensional (1D) ^{13}C and ^{31}P NMR spectra were recorded with either cross-polarization[51] (CP) from ^{1}H nuclei to ^{13}C or ^{31}P nuclei (Fig. S2A,B) or direct pulsing (DP) of ^{13}C or ^{31}P nuclei (Fig. S2C). Typically, the ^{1}H rf amplitude was 66 kHz and the ^{13}C or ^{31}P rf amplitude was ramped linearly from 49 to 59 kHz during the CP contact time. The CP echo sequence in Fig. S2B was used in some cases to minimize baseline distortions in 1D spectra from rf pulse ring-down. 1D ^{13}C NMR spectra were also recorded with the "insensitive nuclei enhanced by polarization transfer" (INEPT) technique[52] (Fig. S2D), using a total polarization transfer period of 4.8 ms. ^{1}H decoupling amplitudes were typically 88 kHz in CP and DP measurements, with two-pulse phase modulation[53] (TPPM) during signal acquisition periods. Decoupling amplitudes were 10 kHz in INEPT measurements, with composite pulse decoupling[54] based on a 125-pulse composite π sequence[55].

As is well-known, CP-based spectra depend on strong magnetic dipole-dipole couplings to ^{1}H nuclei and therefore show strong signals only from sites with restricted mobility. INEPT-based spectra depend on weaker scalar couplings (J couplings) to ^{1}H nuclei. Therefore, under our measurement conditions of moderate-speed MAS and low-power ^{1}H decoupling, INEPT-based spectra show signals only from sites that undergo rapid, nearly isotropic molecular motions. In principle, all sites contribute to DP-based spectra, regardless of mobility.

For quantitative 1D ^{13}C and ^{31}P spectra, recycle delays were adjusted based on measurements of ^{1}H, ^{13}C, ^{31}P spin-lattice relaxation times. Recycle delays were 4-8 s for ^{13}C CP spectra, 2-25 s for ^{13}C DP spectra, 2-12 s for ^{31}P CP spectra, and 7-1000 s for ^{31}P DP spectra.

Two-dimensional (2D) ^{13}C-^{13}C NMR spectra of MBPA-C-FG30 samples that show signals from sites with restricted mobility were recorded with ^{1}H-^{13}C CP and a 30 ms dipolar-assisted rotational resonance[56] (DARR) mixing period for ^{13}C-^{13}C polarization transfers (Fig. S2E). For

measurements at 14.1 T, the recycle delay was 1.0 s, 128 complex t_1 points were acquired with a 25.0 μs t_1 increment, and 256 or 512 scans were taken per complex t_1 point. For measurements at 17.5 T, the recycle delay was 2.0 s, 160 complex t_1 points were acquired with a 20.0 μs t_1 increment, and 768 scans were taken per complex t_1 point. 2D ^{1}H-^{13}C NMR spectra that show signals from highly mobile sites were acquired with ^{1}H-^{13}C INEPT (Fig. S2F), a 1.0 s recycle delay, 64 complex t_1 points with a 100.0 μs t_1 increment, and 512 scans per complex t_1 point. 2D ^{13}C-^{13}C NMR spectra that show signals from highly mobile sites were acquired with ^{1}H-^{13}C INEPT and with ^{13}C-^{13}C polarization transfers driven by scalar couplings in a 12.5 ms "total correlation spectroscopy" (TOCSY) mixing period[57] (Fig. S2G). During the mixing period, ^{13}C chemical shift differences were removed by applying a 125-pulse composite pulse sequence[55] twice, with a 10 kHz ^{13}C rf amplitude. The recycle delay was 1.0 s, 64 complex t_1 points were acquired with a 100.0 μs t_1 increment, and 512-864 scans were taken per complex t_1 point.

Site-specific ^{1}H and ^{13}C spin relaxation times were measured from the dependence of resolved ^{13}C NMR signals on relaxation periods t_{rel}. ^{1}H spin-lattice relaxation times T_1^H, rotating-frame relaxation times $T_{1\rho}^H$, and transverse relaxation times T_2^H were measured by inversion-recovery during t_{rel}, spin-locking decay along a 10 kHz field during t_{rel}, or spin-echo decay during t_{rel}, respectively, followed by INEPT transfers to ^{13}C nuclei for signal detection (Figs. S2H-S2J). ^{13}C spin-lattice relaxation times T_1^C were measured by inversion-recovery during t_{rel}, followed by spin-echo detection (Fig. S2K). ^{13}C transverse relaxation times T_2^C were measured by spin-echo decay during t_{rel}. To avoid spin-echo modulation due to ^{13}C-^{13}C scalar couplings, a Gaussian-shaped, frequency-selective π pulse (2.35 ms pulse length) was used in T_2^C measurements, with a ^{13}C carrier frequency offset Δf that was adjusted to select signals from individual sites or groups of sites (Fig. S2L). Recycle delays were 2.0 s in all relaxation measurements.

^{13}C chemical shifts are relative to 4,4-dimethyl-4-silapentane-1-sulfonic acid, using the $^{13}C_\alpha$ line of L-valine powder at 63.46 ppm as an external standard. ^{31}P chemical shifts are relative to phosphoric acid, using the ^{31}P line of aminomethyl phosphonic acid (AMPA) at 18.8 ppm as an external standard[58]. 1D spectra were processed, analyzed, and plotted with Tecmag TNMR software. 2D spectra were processed and plotted with nmrPipe software[59].

Nuclear spin relaxation data were analyzed with GraphPad Prism 10. In most cases, signal amplitudes $A(t_{rel})$ were measured from peak heights in 1D ^{13}C NMR spectra and uncertainties were set equal to the root-mean-squared (RMS) noise in the spectra. For relaxation measurements on unresolved backbone CO signals and unresolved signals from F19 aromatic sites C2-C6, signal amplitudes were measured as peak areas and uncertainties were set equal to the RMS values of noise areas, using the same frequency ranges to calculate all areas. In all cases, the build-up or decay of signal amplitudes with increasing t_{rel} was fit initially with a single-exponential function, *e.g.*, $A(t_{rel}) = a + b\exp(-t/T_1^H)$. We considered the resulting single-exponential fit to be adequate if the reduced χ^2 value reported by the GraphPad software was less than 2.0. If the single-exponential fit was not adequate ($\chi^2 > 2.0$), we then used a stretched-exponential function to determine the relaxation time, *e.g.*, $A(t_{rel}) = a + b\exp[-(t/T_1^H)^\beta]$ with the additional parameter β. If a stretched-exponential function was required to fit a given relaxation measurement for a given site at any temperature, then stretched-exponential functions were used at all temperatures.

Electron microscopy

Transmission electron microscope (TEM) images were acquired with an FEI Morgagni

microscope, operating at 80 kV, and a side-mounted Advantage HR camera (Advanced Microscopy Techniques). TEM grids were lacey carbon on 300 mesh copper (Electron Microscopy Sciences), upon which carbon films were deposited by flotation. Solutions containing aggregated MBPA-C-FG30 were diluted 100-fold in H_2O, then adsorbed in 10 µl aliquots to glow-discharged grids for 90 s. Grids were blotted, rinsed with H_2O, blotted, rinsed again, blotted, and stained with 2% w/v uranyl acetate for 15 s before final blotting and drying in air.

Scanning electron microscope (SEM) images of AAO20 wafers were acquired with a Hitachi S-4800 field emission SEM instrument. Fragments of wafers were mounted on carbon-based conductive adhesive tape and further immobilized using ultraviolet-curable adhesive (Loctite AA 3494) to minimize drift during imaging, then coated with 1 nm of gold by argon plasma sputtering. The accelerating voltage was set to 1.0 keV. The detection mode in the Hitachi software was set to "L.A. 1" for a combination of secondary electron and low-angle back-scattered electron detection.

Atomic force microscopy

Atomic force microscope (AFM) images were acquired in tapping mode with a Veeco Multimode instrument with Nanoscope IV controller, using a Nanosensors PPP-NCHAuD probe with 320 kHz resonant frequency. Images were recorded at 7.96 µm/s tip velocities with 512 × 512 points and 1.0 µm × 1.0 µm nominal dimensions. Image dimensions were corrected by measurements on a standard calibration grid.

Optical and fluorescence microscopy

For confocal fluorescence microscopy, FITC-labeled MBPA-C-FG30-4G (prepared as described above) was dissolved in Bis-Tris buffer (0.2 M, pH 6.5) to obtain a 1.0 mM solution. This solution was then diluted 40-fold with a 1.0 mM solution of unlabeled MBPA-C-FG30-4G in the same buffer to reduce the FITC density. H_2SO_4-treated AAO20 wafer samples (~3 mg each) were incubated in 200 µl of the diluted solution in 0.5 ml tubes at 40° C with rotation and shaking. Four wafers were processed in parallel, each in a separate tube, with incubation times of 10 min, 1 h, 3 h, and 24 h. After incubation, wafer samples were washed in DMSO for 10 minutes, followed by three 10-minute washes with deionized water.

For control experiments, wafer pieces were incubated quiescently at 24° C for 10 min and 30 min in solutions containing 50 µg/ml fluorescein and 6 M guanidine hydrochloride (GuHCl), followed by rinsing with water. GuHCl was included to reduce adsorption of fluorescein to AAO20 surfaces, which otherwise resulted in high fluorescein densities that interfered with confocal fluorescence imaging. The fluorescein solution was prepared by diluting a 1 mg/ml fluorescein stock solution in DMSO with GuHCl/Bis-Tris buffer to the desired concentration. All prepared wafers were stored in water and kept in the dark until shortly before confocal imaging.

Confocal fluorescence imaging was performed with a Zeiss LSM 780 microscope equipped with a Plan-Apochromat 100x/1.40 Oil DIC objective lens. AAO20 wafer pieces were imaged in water-filled 35 mm glass-bottom microwell dishes (MatTek Corporation). Wafer pieces were covered by 12 mm circular cover glass (Erie Scientific Company), with an additional metal O-ring on top of the cover glass to keep the wafer in position during imaging. Fluorescence was excited with a 405 nm laser and collected with a 514 – 585 nm emission filter. The pinhole was set to 1.31 Airy units and z-stacks were acquired at 1.0 µm intervals. No refractive index corrections were

applied. Imaging parameters were kept constant for all samples. To generate plots of fluorescence intensity as a function of z (the direction parallel to AAO20 pores), Fiji software[60] was used to calculate the average intensity in each slice of the confocal z-stack, averaging over the entire field of view in each slice.

Bright-field optical images of AAO20 wafers were recorded with an Olympus BX50 microscope, equipped with a SPOT Idea camera.

RESULTS

Characterization of starting materials by NMR and microscopy

For comparison with spectra of MBPA-C-FG30 samples under other conditions described below, Fig. 2 shows solid state NMR spectra of purified MBPA-C-FG30-LSAFTG in the form of a lyophilized powder. These spectra were acquired with MAS at 12.00 kHz, cross-polarization from ^{1}H spins[51], and high-power ^{1}H decoupling during signal acquisitions[53]. NMR lines in the one-dimensional (1D) ^{13}C and ^{31}P spectra (Fig. 2A) are inhomogeneously broadened, consistent with a conformationally disordered and rigid state. The two-dimensional (2D) ^{13}C-^{13}C spectrum (Fig. 2B), acquired with a 30 ms DARR mixing period[56], shows strong intra-residue crosspeaks, with full-width-at-half-maximum (FWHM) linewidths in the 1-5 ppm range, that can be assigned to individual residues based on their connectivity patterns and the expected residue-specific chemical shift ranges. Table 1 lists ^{13}C chemical shift values and linewidths from the 2D spectrum in Fig. 2B and from other spectra described below.

AAO wafers with 13 mm diameter, 50 μm thickness, and 20 ± 3 nm diameter pores were obtained from InRedox LLC (part number AAO-013-020-050, subsequently called AAO20). Figs. 3A and 3B show SEM and AFM images of AAO20 wafers as received. Images of the wafer surfaces show a pseudo-regular pattern of pores with an average density of 467 ± 69 pores/μm^2 (482 ± 31 pores/μm^2 from four AFM images with approximately 0.7 μm^2 area in each image; 435 ± 91 pores/μm^2 from five SEM images with approximately 1.0 μm^2 area in each image). SEM images of fractured edges of AAO20 wafers show the expected straight pores, with diameters that are consistent with the expected 20 nm value to within the image resolution.

With a 20 nm pore diameter, the average pore density seen in SEM and AFM images implies a porosity value (*i.e.*, fraction of wafer volume occupied by pores) equal to 14.7 ± 2.2%. Assuming smooth pore walls, a 13 mm wafer diameter, and a 50 μm wafer thickness, the calculated surface area per within pores is $(1.95 \pm 0.29) \times 10^5$ mm^2 per wafer. In contrast, the area of the exterior surfaces of the wafer is only 230 mm^2. If molecules could be attached to the pore walls of AAO20 with an average spacing of 1 nm between molecules, these calculations suggest that one wafer could hold approximately 0.3 μmole of molecules, a quantity that is easily sufficient for NMR measurements.

We also estimated the porosity of AAO20 wafers more directly by weighing dry wafers, soaking them in H_2O, quickly blotting them with filter paper, and weighing them again within 5 s of removal from H_2O. These measurements were performed three times on each of three AAO20 wafers. Assuming that mass differences between dry and hydrated states were due to H_2O that completely filled the pores in wafers with 13 mm diameter and 50 μm thickness (6.64 μl volume), we derived a porosity value of 16.3 ± 1.0%, in good agreement with the value estimated from SEM and AFM images.

^{31}P NMR spectra of untreated AAO20 revealed the unanticipated presence of a relatively

large signal (Fig. S3A). By comparing the ^{31}P signal area from untreated AAO20, recorded with direct pulsing of ^{31}P polarization, with the ^{31}P signal area from a known mass of ammonium phosphate, we estimated that one wafer of AAO20 contained approximately 1.2 μmol of phosphorus. If this phosphorus resides on surfaces, it corresponds to a surface density of 4 nm^{-2}, using the surface area calculated above, which could interfere with the attachment of MBPA-C-FG30 to AAO20 pore surfaces. Following a suggestion from Dr. Dmitri Routkevitch of InRedox LLC, we found that brief treatments with 0.1 M H_2SO_4 can be used to remove residual surface phosphates without increasing the AAO pore diameters significantly. ^{31}P NMR data in Fig. S3 demonstrate the effectiveness of these treatments. Brief H_2SO_4 treatments had no discernible effect on AFM images of AAO20 (Fig. 3D).

Finally, to determine appropriate conditions for incubation of AAO20 with MBPA-C-FG30, we examined the effects on AAO20 of incubation at 40° C in aqueous buffers with pH values between 0.4 and 14.7. After 94 h incubation periods at pH values below 6.2 or above 8.1, AAO20 wafer samples were obviously damaged, dissolving or losing their normal transparency (Fig. S4). Based on these observations, subsequent incubation experiments were performed with 0.2 M Bis-Tris buffer, pH 6.5 (except as noted). SEM images (Fig. 3C) confirmed that the nanoporous structure of AAO20 was retained after brief treatments with 0.1 M H_2SO_4 and incubation in 0.2 M Bis-Tris buffer, pH 6.5, at 40° C for 24 h. Additionally, NMR results described below show that MBPA-C-FG30/AAO20 samples remain stable in 0.2 M Bis-Tris buffer, pH 6.5, during many weeks of measurements over a wide temperature range.

Optimization of FG30 attachment in AAO nanopores

To attach MBPA-C-FG30 peptides to pore surfaces in AAO20, AAO20 wafers or wafer pieces were incubated at 40° C in 1.0 mM solutions of MBPA-C-FG30 in 0.2 M Bis-Tris buffer, pH 6.5. Incubations were performed in a temperature-controlled tube rotator (Roto-Therm Mini Plus, Benchmark Scientific). Typically, 1.0 ml of solution was contained in a 1.5 ml tube, with end-over-end rotation at 30 revolutions per minute and intermittent shaking in each rotation cycle. After incubation, the AAO20 material was rinsed with three successive 1.5 ml volumes of deionized water, then dried overnight under a stream of nitrogen gas. The dried material was crushed into small pieces, approximately 0.5-2 mm in diameter, and packed into MAS rotors for NMR measurements.

Figs. 4A and 4B show 1D ^{13}C and ^{31}P NMR spectra of dry samples of MBPA-C-FG30-LSAFTG/AAO20 and MBPA-C-FG30-4G/AAO20. The absence of sharp lines from H_2O in ^{1}H NMR spectra of these samples confirmed their dryness. From saturation-recovery measurements, spin-lattice relaxation times for ^{1}H, ^{13}C, and ^{31}P nuclei in these dry samples (T_1^H, T_1^C, T_1^P) were determined to be approximately 0.6 s, 1.5 s (LSAFTG) or 30 s (4G), and 200 s, respectively. Similar spectra were obtained for samples prepared with a variety of incubation conditions (Figs. S5 and S6), using recycle delays greater than three times the relevant T_1^H or T_1^C values. Aliphatic ^{13}C and ^{31}P signal areas in these spectra were measured, normalized by the number of scans in each spectrum, and compared with signal areas in ^{13}C NMR spectra of 1.25 mg of uniformly ^{15}N,^{13}C-labeled L-valine powder (10.1 μmol of L-valine, 40.6 μmol of aliphatic ^{13}C) and 5.0 mg of aminomethyl phosphonic acid (AMPA) powder (45.0 μmol of ^{31}P) (Fig. S7). The resulting estimates of the loading of MBPA-C-FG30 in AAO20 are listed in Table 2. In most cases, estimates of loading from ^{13}C CP, ^{13}C DP, and ^{31}P CP signal areas are in good agreement for each sample, with discrepancies attributable to limited signal-to-noise ratios and uncertainties regarding

baseline corrections in the spectra.

Variations in incubation conditions for the first 11 samples in Table 2 included variations in incubation times, substitution of 25 mM acetate buffer for 0.2 M Bis-Tris buffer (sample 9 only), use of AAO with 40 nm pores (sample 3 only), incubation of three wafers in a single tube containing 1.0 ml of 1.0 mM MBPA-C-FG30 solution rather one wafer per tube (samples 2, 6, and 7), and crushing of AAO20 into small pieces prior to incubation (sample 7 only). Incubation times greater than 24 h did not produce higher loading values. Loading values with 1.0 ml of peptide solution per wafer were higher than with 0.33 ml of solution per wafer. Crushing of AAO20 prior to incubation did not increase the loading. Similar results were obtained with acetate and Bis-Tris buffers.

Based on the results in Table 2, a final MBPA-C-FG30-LSAFTG/AAO20 sample was prepared by incubating three intact wafers in separate tubes for 24 h, with 1.0 ml of peptide solution in each tube. After thorough rinsing and drying, this sample (sample 12 in Table 2) was determined to contain 5.8 ± 0.1 nmol/mg of MBPA-C-FG30-LSAFTG, with 0.27 μmol of MBPA-C-FG30-LSAFTG in the MAS rotor. Measurements of dynamics and effects of hydration described below were performed on this sample.

Given the 15% porosity value discussed above and the 3.3 kDa molecular weight of MBPA-C-FG30, the average peptide concentration within AAO20 nanopores in sample 12 is about 90 mM or 300 mg/ml. Assuming a density of 1.4 g/ml for the peptide[61], about 21% of the AAO20 pore volume is filled by MBPA-C-FG30 molecules, on average.

As a simple test for the uniformity of MBPA-C-FG30 density within AAO20 pores, we obtained AAO20 flakes with 5 μm thickness from InRedox LLC. We prepared MBPA-C-FG30-4G/AAO20 from this thinner material, using the same conditions described above for H_2SO_4 treatment, incubation in 1.0 mM MBPA-C-FG30-4G at 40° C for 24 h, rinsing with deionized water, and drying. The signal area in the cross-polarized ^{13}C NMR spectra of 4.9 mg of the final dried material indicated a loading of 5.13 ± 0.33 nmol per mg (sample 4 in Table 2 and Fig. S5), nearly the same as the loading of standard wafers with 50 μm thickness. This result is consistent with nearly uniform peptide densities in the AAO20 pores. Additional measurements of density distributions in AAO20 pores, based on confocal fluorescence microscopy, are described below.

Effects of hydration on FG30 conformation and dynamics in AAO nanopores

Fully hydrated states of MBPA-C-FG30/AAO20 samples were created by adding 0.2 M Bis-Tris buffer, pH 6.5, to the MAS rotors. The rotors were tightly sealed with cyanoacrylate glue, as verified by periodic measurements of the intensities of ^{1}H NMR signals from liquid water throughout the experiments described below. In this context, it is worth emphasizing that AAO wafers are inherently hydrophilic, rapidly absorbing water and becoming almost fully transparent to visible light as the nanopores fill with water.

As shown in Fig. 4C, hydration has a dramatic effect on ^{13}C NMR spectra of MBPA-C-FG30-LSAFTG/AAO20 and MBPA-C-FG30-4G. Directly-pulsed ^{13}C NMR signals become sharper (0.15 ppm FWHM linewidths for doublet components of the Thr22 $^{13}C_{\gamma}$ line at 20° C) while retaining the same signal areas as in the dry state (ratio of areas equal to 1.00 ± 0.05 for signals between 80 ppm and 0 ppm). Cross-polarized ^{13}C signals become weak, with the total aliphatic signal area being reduced by a factor of approximately 18 relative to the dry state. Moreover, in the hydrated state it becomes possible to observe strong, sharp ^{13}C NMR signals from aliphatic sites after polarization transfer from ^{1}H spins with the INEPT technique[52] and with low-

power ^{1}H decoupling. These observations show that FG30 peptide chains become highly dynamic within water-filled AAO20 nanopores, executing large-amplitude motions on submicrosecond time scales that strongly attenuate magnetic dipole-dipole couplings among nuclei. Molecular motions in the hydrated state also average out the local conformational and environmental differences that lead to inhomogeneously broadened NMR lines in the dry state.

In contrast to the ^{13}C NMR signals, ^{31}P NMR signals from MBPA-C-FG30-LSAFTG/AAO20 are not strongly affected by hydration, with linewidths and signal areas in cross-polarized spectra being nearly equal in dry and hydrated states (Fig. 4B). This observation is consistent with covalent bonding of the MBPA phosphonate group to the AAO20 nanopore wall surfaces, which renders the phosphonate group immobile regardless of hydration. In contrast, if MBPA-C-FG30 was associated with AAO20 without covalent bonding between MBPA phosphonates and nanopore walls, one would expect the ^{31}P NMR linewidth to be reduced by molecular motions in the hydrated state (as observed for the ^{13}C NMR linewidths in Fig. 4C).

Fig. 5 shows 2D NMR spectra of the same MBPA-C-FG30-LSAFTG/AAO20 sample, including a 2D ^{13}C-^{13}C spectrum of the dry sample obtained with ^{1}H-^{13}C cross-polarization, high-power ^{1}H decoupling in t_1 and t_2 periods, and a 30 ms DARR mixing period (Fig. 5A), a 2D ^{13}C-^{13}C spectrum of the hydrated sample obtained with ^{1}H-^{13}C INEPT, low-power ^{1}H decoupling in t_1 and t_2 periods, and a 12.5 ms isotropic mixing (TOCSY) period (Fig. 5B), and a 2D ^{1}H-^{13}C spectrum of the hydrated sample obtained with ^{1}H-^{13}C INEPT and low-power ^{1}H decoupling in the t_2 period (Fig. 5C). All 2D spectra in Fig. 5 were acquired at 20° C. The 2D ^{13}C-^{13}C spectrum of the dry sample in Fig. 5A resembles the 2D ^{13}C-^{13}C spectrum of lyophilized MBPA-C-FG30-LSAFTG in Fig. 2B, but with significant differences in positions and intensities of crosspeaks that suggest differences in peptide conformational distributions between the dry, AAO20-bound state and the lyophilized state. Crosspeak widths are greatly reduced in the 2D ^{13}C-^{13}C and 2D ^{1}H-^{13}C spectra of the hydrated sample in Figs. 5B and 5C (<0.6 ppm for ^{13}C, limited by pulse sequence conditions, 0.10 ppm for ^{1}H).

Chemical shifts from 2D spectra in Figs. 2 and 5 are listed in Table 1. In the hydrated state, ^{1}H and ^{13}C chemical shifts are nearly identical to random-coil values[62], consistent with rapid exchange within a broad distribution of conformations. In the dry, AAO20-bound state and the lyophilized state, ^{13}C chemical shifts measured at the centers of inhomogeneously broadened crosspeaks deviate more strongly from random-coil values.

Temperature dependence of FG30 conformation and dynamics in AAO nanopores

To test for a possible temperature dependence of conformational preferences in hydrated MBPA-C-FG30-LSAFTG/AAO20, we recorded 1D ^{13}C NMR spectra at temperatures between -5° C and 50° C. Spectra recorded with direct pulsing of ^{13}C spins show sharper lines at 50° C than at lower temperatures, but total signal areas are independent of temperature to within experimental error (Fig. S8A). Spectra recorded with ^{1}H-^{13}C INEPT show sharper lines and larger signal areas at higher temperatures, indicating greater ^{1}H-^{13}C polarization transfer efficiencies at higher temperatures due to reductions in transverse spin relaxation rates (Fig. S8B). Temperature-dependent changes in ^{13}C chemical shifts are less than 0.1 ppm for most ^{13}C-labeled sites, except that the chemical shifts of the $C_{\delta1}$ and $C_{\delta2}$ sites of L6, the C_{β} sites of S11 and A16, the C_{γ} site of T22, and the C_{α} site of G28 increase by 0.25-0.66 ppm with increasing temperature. The A16 C_{β} site shows the largest change with temperature (0.66 ppm from -5° C to 50° C). For comparison, Kjaergaard *et al*. report a 0.0047 ppm per degree temperature dependence of the random-coil C_{β}

site of alanine[63]. These results show that conformational preferences of MBPA-C-FG30 are not strongly temperature-dependent in the AAO20-bound, hydrated state.

Signals in spectra recorded with ^{1}H-^{13}C cross-polarization are generally weaker than in spectra recorded with direct pulsing, indicating inefficient cross-polarization due to attenuation of ^{1}H-^{13}C dipole-dipole couplings by molecular motions (Fig. S8C). From -5° C to 50° C, the ratio of the total aliphatic signal area per scan in cross-polarized spectra to the total aliphatic signal area per scan in directly-pulsed spectra decreases from 0.48 ± 0.07 to 0.21 ± 0.03. The fact that signals in cross-polarized ^{13}C spectra do not drop to zero at high temperatures indicates that rapid motions in MBPA-C-FG30-LSAFTG/AAO20 are not fully isotropic for all peptide molecules. At 50° C, the strongest signals in the cross-polarized ^{13}C spectrum arise from aliphatic carbons of Leu6, the labeled residue that is closest to the point of attachment to the nanopore wall, where molecular motions are likely to be most restricted (Fig. S8C).

2D ^{13}C-^{13}C and ^{1}H-^{13}C spectra, with polarization transfers driven by scalar couplings, also show larger crosspeak intensities and sharper crosspeaks at higher temperatures but are otherwise nearly independent of temperature (Fig. S9).

To probe molecular motions in more detail, we measured the temperature dependences of five nuclear spin relaxation times from -5° C to 50° C, namely the ^{1}H and ^{13}C spin-lattice relaxation times T_1^H and T_1^C (pulse sequences in Figs. S2H and S2K), the ^{1}H and ^{13}C transverse relaxation times T_2^H and T_2^H (pulse sequences in Figs. S2J and S2L), and the ^{1}H rotating-frame relaxation time $T_{1\rho}^H$ (pulse sequence in Fig. S2I). All relaxation times were measured as build-up or decay times of ^{13}C signals, allowing separate measurements for sites with resolved lines in 1D ^{13}C spectra. ^{1}H relaxation times were measured through ^{13}C signals after INEPT polarization transfers. T_2^C values were measured from spin echo decays, using frequency-selective ^{13}C π pulses to minimize effects of ^{13}C-^{13}C scalar couplings.

Fig. 6 shows examples of spin relaxation data and the temperature dependences of relaxation times extracted from these data. The full sets of data appear in Figs. S10-S14. Values of relaxation times were extracted from these data by fitting with single-exponential or, in cases where single-exponential fits were deemed inadequate (see Materials and Methods), stretched-exponential functions. Best-fit parameters for all relaxation data are given in Tables S1-S5. Values of the best-fit stretching parameter β greater than 1.0 in the case of T_2^C data for F19 aromatic sites are attributable to effects of ^{13}C-^{13}C scalar couplings among aromatic carbons. Plots of the temperature dependences of all measured relaxation times appear in Figs. S15-S19.

All T_1^H values are in the 0.3-0.6 s range and nearly independent of temperature (Fig. S15). T_1^C values are in the 0.2-0.6 s range, either increasing or decreasing by less than 30% between -5° C and 50° C for most sites (Fig. S18). T_1^C of the T22 C_γ site has the strongest temperature dependence, increasing by 50%. T_2^H values for methyl sites (Leu6 $C_{\delta 1}$ and $C_{\delta 2}$, Ala16 C_β, Thr22 $C\gamma$) and for the Phe19 sidechain increase by factors of roughly 2-3 with increasing temperature, while other T_2^H values are more weakly temperature-dependent (Fig. S17). In contrast, T_2^C values for most sites increase by factors of 3-6 with increasing temperature, with smaller increases only for the Phe19 sidechain sites (Fig. S19).

T_2^C values for the A16 C_β and T22 C_γ sites have apparent sigmoidal dependences on temperature (Fig. S19), increasing by factors of 2.8 and 3.2 from 20° C to 30° C. These are the only two relaxation times whose temperature dependences are not adequately described by the second-order polynomial functions used as guides to the eye in Figs. 6 and S15-S19. Although the increase in T_2^C values for the A16 C_β and T22 C_γ sites between 20° C and 30° C suggests an approximate three-fold reduction in orientational correlation times for methyl axis directions at

these sites around 25° C, the absence of similar increases in T_2^C values for A16 C_α and T22 C_β sites argues against such an interpretation.

$T_{1\rho}^H$ values for most sites exhibit non-monotonic temperature dependences, with minima at temperatures in the 10-30° C range (Fig. S16). T_2^H values for some sites (S11 C_β, A16 C_α, F19 C_β, G28 C_α, and the combined signal from S11 C_α and F19 C_α) have similar non-monotonic temperature dependences. For these sites, $T_{1\rho}^H \approx T_2^H$ near 25° C, but values of $T_{1\rho}^H$ are 1.5-2.0 times large than values of T_2^H at the highest and lowest temperatures. T_2^H values for the aromatic sidechain sites of F19 are smaller than $T_{1\rho}^H$ values over the entire temperature range and increase monotonically with increasing temperature, suggesting a role for slow sidechain ring motions. Slow ring motions may also determine the temperature dependence of T_2^C for F19 sidechain sites. T_2^H values for the T22 C_γ site increase monotonically, are smaller than $T_{1\rho}^H$ values at the highest and lowest temperatures, but are larger than $T_{1\rho}^H$ values at 10° C and 20° C. T_2^H values for the L6 $C_{\delta1}$ and $C_{\delta2}$ sites increase monotonically, becoming larger than $T_{1\rho}^H$ values above 5° C.

An important conclusion from these relaxation measurements is that the collection of MBPA-C-FG30 molecules within an AAO20 nanopore does not undergo a temperature-driven phase transition in the range from -5° C to 50° C, since phase transitions generally produce changes in molecular motions that would produce discontinuities in the temperature dependences of spin relaxation times[64-65]. The possibility of a phase transition is suggested by experimental studies of phase-separated droplets and hydrogels formed by FG-repeat domains in free solution[32-35]. In particular, the relaxation data and the temperature-dependent NMR spectra (Figs. S8 and S9) rule out a transition between a state in which peptide chains move independently of one another and a state in which neighboring peptide chains form long-lived clusters or cohesive assemblies through intermolecular contacts with microsecond or longer lifetimes. Formation of long-lived clusters above or below a specific transition temperature would be expected to produce a sudden broadening of NMR lines and reduction in $T_{1\rho}^H$, T_2^H, and T_2^C values. Rather than a phase transition, our data indicate continuous increases in molecular mobility (*i.e.*, reductions in correlation times for molecular motions) with increasing temperature.

We have not attempted a quantitative analysis of the relaxation data due to the complexity of coupled spin dynamics in methylene and methyl groups, complications due to ^{1}H-^{1}H cross-relaxation, and the likely complexity of molecular motions in hydrated MBPA-C-FG30/AAO20. As an example, the experimentally determined relaxation times for the Ala16 C_α site illustrate the inadequacy of a simple treatment. If this site acts as an isotropically tumbling, dipole-coupled, two-spin ^{1}H-^{13}C system, standard expressions for the relaxation times[66] could conceivably apply:

$$1/T_1^X = \frac{d^2\tau_c}{10}\{[1+(\omega_X-\omega_Y)^2\tau_c^2]^{-1}+3[1+\omega_X^2\tau_c^2]^{-1}+6[1+(\omega_X+\omega_Y)^2\tau_c^2]^{-1}\} \quad (1a)$$

$$1/T_2^X = \frac{d^2\tau_c}{20}\{4+[1+(\omega_X-\omega_Y)^2\tau_c^2]^{-1}+3[1+\omega_X^2\tau_c^2]^{-1}+6[1+\omega_X^2\tau_c^2]^{-1} +6[1+(\omega_X+\omega_Y)^2\tau_c^2]^{-1}\} \quad (1b)$$

In Eqs. (1), X and Y are either H and C, respectively, or C and H. NMR frequencies in rad/s are ω_X and ω_Y. The orientational correlation time is τ_c. Assuming a 0.11 nm ^{1}H-^{13}C distance, the dipole-dipole coupling constant d is 3.58×10^4 rad/s. Given that $T_1^H \approx T_1^C \approx 0.5$ s for the Ala16 C_α site at 20° C (Figs. S15 and S18; Tables S1 and S3), Eq. (1a) implies $\tau_C \approx 0.1$ ns. However,

according to Eq. (1b), the measured values $T_2^H \approx 11$ ms and $T_2^C \approx 9$ ms (Figs. S17 and S19; Tables S4 and S5) imply $\tau_C \approx 22$ ns and $\tau_C \approx 27$ ns, respectively. In addition, the three-fold increase in T_2^C from 20° C to 50° C suggests a three-fold decrease in τ_c, inconsistent with the nearly constant values of T_1^H, T_2^H, and T_1^C over the same temperature range if Eqs. (1) were valid.

The failure of Eqs. (1) to explain the experimental data, even approximately, implies that distinct motions with distinct temperature-dependent amplitudes and correlation times contribute to various relaxation rates. At a qualitative level, relaxation data for the Ala16 C_α site may be explained by a combination of sub-nanosecond, limited-amplitude motions of the C_α-H_α bond direction due to rapid local conformational fluctuations and slower, nearly-isotropic motions of the C_α-H_α bond direction due to global conformational rearrangements, with the time scale for global motions becoming shorter with increasing temperature. Relaxation data for other sites may be explained similarly, with additional effects due to methyl rotation, aromatic ring flips, and exchange among sidechain rotamers.

Aggregation of FG30 in free solution

Results presented above show that MBPA-C-FG30 molecules are highly dynamic in aqueous solution at concentrations near 90 mM and over a wide temperature range when tethered to the nanopore walls of AAO20. Sharp lines and random-coil chemical shifts in NMR spectra (Figs. 4C, 5B, and 5C; Table 1) indicate the absence of oligomerization or aggregation, and no spectral changes occur over many weeks of measurements. In contrast, untethered MBPA-C-FG30 aggregates at 10 mM concentration in 0.2 mM Bis-Tris buffer, pH 6.5 when incubated at 4° C, 24° C, or 37° C. Negative-stain TEM images in Fig. 7, after six days of incubation, show that the aggregated material consists of straight, unbranched assemblies with morphologies and dimensions typical of amyloid fibrils[11, 17, 22].

To estimate the equilibrium solubility of MBPA-C-FG30, 7.1 mM solutions in the same buffer (23 mg/ml, 50-140 µl volumes) were incubated at 4° C, 24° C, and 40° C for four days, with brief bath sonication (10-15 s) once per day to accelerate the approach to equilibrium. After incubation, solutions were centrifuged at 16,000 × g for 15 min, yielding visible pellets at each temperature. Supernatants were then passed through 0.1 µm centrifugal filters (Millipore Ultrafree, 0.5 ml volume) and diluted with H_2O by factors of four. Peptide concentrations were determined from absorbance measurements at 260 nm, performed in triplicate, using an extinction coefficient of 1070 M^{-1} cm^{-1} that was determined from the absorbance of the initial solutions. Based on these measurements, equilibrium solubilities of MBPA-C-FG30 in 0.2 mM Bis-Tris buffer, pH 6.5, are 4.5 ± 0.2 mM, 1.60 ± 0.04 mM, and 1.92 ± 0.08 mM at 4° C, 24° C, and 40° C. Thus, the concentration at which MBPA-C-FG30 remains unaggregated and apparently monomeric when tethered to nanopore walls of AAO20 greatly exceeds the equilibrium solubilities in free solution.

Figs. 8A and 8B show cross-polarized 1D ^{13}C and directly-pulsed 1D ^{31}P NMR spectra of aggregated MBPA-C-FG30-LSAFTG, prepared by incubation of a 10 mM solution at 24° C. Fig. 8C shows a 2D ^{13}C-^{13}C NMR spectrum, obtained with ^{1}H-^{13}C CP, a 30 ms DARR mixing period, and high-power ^{1}H decoupling. For these measurements, aggregated material was pelleted by ultracentrifugation (278000 × g, 120 min, 20° C), then transferred by centrifugation into the MAS NMR rotor without lyophilization or drying. The aggregated material was therefore fully hydrated with 0.2 M Bis-Tris buffer, pH 6.5. Although the 1D ^{13}C and 2D ^{13}C-^{13}C spectra in Fig. 8 were obtained with NMR measurement conditions appropriate for immobilized molecules, signals are

sharp (0.6-1.0 ppm FWHM linewidths), consistent with an ordered peptide conformation and only small-amplitude motion at the ^{13}C-labeled sites in the aggregated state (except for the aromatic sidechain of Phe19, from which signals are weak). Aliphatic signal areas in 1D ^{13}C NMR spectra obtained with direct pulsing or with ^{1}H-^{13}C INEPT were 1.7 or 3.8 times smaller, respectively, than the aliphatic signal area in Fig. 8A.

The ^{31}P linewidth in Fig. 8B is 20 times smaller than the ^{31}P linewidth for hydrated MBPA-C-FG30-LSAFTG/AAO20 in Fig. 4B. The ^{31}P signal area in the directly-pulsed spectrum is 2.4 times larger than the signal area in a cross-polarized spectrum. In addition, the ^{31}P spin-lattice relaxation time in aggregated MBPA-C-FG30-LSAFTG at 20° C, determined from inversion-recovery measurements, is 0.22 ± 0.02 s, compared with 15 ± 5 s in hydrated MBPA-C-FG30-LSAFTG/AAO20 (Fig. S20). These results indicate that phosphonate groups execute rapid, large-amplitude motions in hydrated, aggregated MBPA-C-FG30. The slow ^{31}P spin-lattice relaxation in MBPA-C-FG30/AAO20 provides additional evidence for covalent bonding of phosphonate groups to AAO nanopore wall surfaces.

The observation of a single set of crosspeaks in the 2D ^{13}C-^{13}C NMR spectrum (Fig. 8C) indicates a homogeneous local structure in aggregated MBPA-C-FG30, despite the morphological heterogeneities in TEM images (Fig. 7). Although the TEM images show amyloid-like fibril morphologies, secondary ^{13}C chemical shifts in Fig. 8D do not support amyloid-like β-strand conformations (typified by negative $^{13}C_{\alpha}$ and ^{13}CO and positive $^{13}C_{\beta}$ secondary shifts) at all labeled residues. Secondary shifts in aggregated MBPA-C-FG30 also differ from those in the lyophilized and AAO20-bound states.

Characterization of FG30 density within AAO nanopores by confocal fluorescence microscopy

To determine the dependence of peptide density on distance from the outer AAO20 surfaces into the nanopores, wafer pieces were incubated in a 1.0 mM MBPA-C-FG30-G solution in which 2.5% of the peptide molecules were fluorescently labeled with FITC. As shown in Fig. 9A, confocal fluorescence microscope images were recorded with excitation at 405 nm and detection at 514-585 nm, using 1.0 μm increments in the distance z perpendicular to the flat wafer surface. Plots of the average fluorescence intensity within the images as a function of z can then be interpreted as plots of peptide density versus z (averaged over directions perpendicular to z, and assuming that FITC-labeled peptide molecules have the same spatial distribution within AAO20 as unlabeled molecules). As shown in Figs. 9B and 9C, the peptide density increases with increasing incubation time. Peptide densities within the nanopores are larger at z values near the two outer surfaces than near the midpoint between these surfaces (z ≈ 25 μm), by factors of 1.4-2.2 after 24 h incubation. Moreover, the peptide densities are not symmetric about the midpoint.

Fluorescence intensity profiles in Figs. 9B and 9C were measured with opposite wafer surfaces directed towards the excitation light (*i.e.*, by flipping the wafer pieces over in their glass-bottom microwell dishes). The fact that the profiles in Figs. 9B and 9C have opposite asymmetries implies that the asymmetries are not due to optical distortions. We speculate that the asymmetries of the fluorescence intensity profiles are a consequence of structural or chemical inequivalence between the two outer surfaces, arising from the inherent asymmetry of the AAO wafer fabrication process[45-46]. The lower fluorescence intensity near the midpoint in these profiles may indicate that diffusion of MBPA-C-FG30 molecules into the midpoint of AAO20 nanopores is impeded by the accumulation of high densities of tethered MPBA-C-FG30 near the two ends of the nanopores. It

is also conceivable that a fraction of the nanopores are not fully open over their entire 50 μm lengths or become partially blocked by extraneous particles in the incubating solutions.

For comparison, Figs. 9D and 9E show fluorescence intensity profiles for AAO20 wafer pieces that were incubated for short times in solutions of fluorescein, which we found to adsorb to the nanopore walls. Although these profiles are not fully symmetric, they do not show minima near z = 25 μm. Thus, small molecules can penetrate through the entire lengths of the nanopores to create a nearly uniform distribution of adsorbed species.

Generality of the approach

To test the applicability of our approach to other peptides in nanopore environments, we incubated 53.0 mg of H_2SO_4-treated AAO20 wafer pieces at 40° C in 0.95 ml of 1.0 mM MBPA-C-melittin-GVA, 50 mM Bis-Tris, pH 6.5 for 50 h. After washing with H_2O and drying under N_2 gas, 1D ^{13}C NMR spectra of the dry MBPA-C-melittin-GVA/AAO20 sample indicated a total of 0.40 ± 0.03 μmoles of peptide in 47.6 mg of crushed AAO20 (0.38 μmole based on the aliphatic signal area in the cross-polarized spectrum in Fig. 10A, 0.43 μmole based on the directly-pulsed spectrum in Fig. 10B). With the 3.2 kDa molecular weight of MBPA-C-melittin-GVA (Fig. S1H), this result implies a peptide concentration of approximately 140 mM (440 mg/ml) in the AAO20 nanopores.

After hydrating the MBPA-C-melittin-GVA/AAO20 sample with 50 mM Bis-Tris, pH 6.5, strong signals were observed in 1D ^{13}C NMR spectra obtained with ^{1}H-^{13}C cross-polarization and with direct pulsing of ^{13}C polarization (Figs. 10C and 10D). Aliphatic signals in a 1D ^{13}C NMR spectrum obtained with ^{1}H-^{13}C INEPT (Fig. 10E) were weaker than in the cross-polarized spectra by a factor of 24. This behavior of hydrated MBPA-C-melittin-GVA/AAO20 is opposite to the behavior of hydrated MBPA-C-FG30-LSAFTG/AAO20, where aliphatic signals in the INEPT ^{13}C NMR spectrum were stronger than signals in the cross-polarized spectrum by an approximate factor of 7 (Fig. 4C). The signal amplitudes in cross-polarized and INEPT spectra indicate that motions of melittin in hydrated MBPA-C-melittin-GVA/AAO20 are restricted, in contrast to the nearly isotropic motions of FG30 in MBPA-C-FG30-LSAFTG/AAO20.

Figs. 10F, 10G, and 10H show 2D ^{13}C-^{13}C NMR spectra of lyophilized C-melittin-GVA, dry MBPA-C-melittin-GVA/AAO20, and hydrated MBPA-C-melittin-GVA/AAO20, respectively. Again in contrast to observations for MBPA-C-FG30-LSAFTG (Figs. 2B, 5A, and 5B, Table 1), crosspeak positions in the three 2D spectra in Fig. 10 are nearly the same, indicating similar peptide conformations. Crosspeaks in the hydrated state of MBPA-C-melittin-GVA/AAO20 are sharper than in the dry state (1.1-1.8 ppm versus 1.5-2.9 ppm FWHM), consistent with rapid but restricted peptide motions, solvation, and rapid solvent diffusion in the hydrated state. Comparison of ^{13}C chemical shifts in Fig. 10H with standard random-coil values[62] indicates an α-helical conformation at the isotopically labeled residues (176.1 and 47.4 ppm for G3; 178.4, 65.9, 31.2, 22.6, and 21.6 ppm for V8; 179.8, 54.6, and 18.2 ppm for A15). Thus, when melittin is tethered to walls of AAO20 nanopores at high concentrations, it adopts an α-helical conformation similar to the known conformation in melittin tetramers in free solution[67-69]. The contrasting behavior of hydrated MBPA-C-melittin/AAO20 and hydrated MBPA-C-FG30/AAO20 implies that the random-coil-like properties of tethered FG30 at high concentrations in AAO20 nanopores are not universal for tethered peptides of similar size at similar concentrations.

Chemical shifts in the 1D INEPT ^{13}C NMR spectrum (Fig. 10E) are close to random-coil values ($^{13}C_{\alpha}$ and $^{13}C_{\beta}$ chemical shifts equal to 62.3 and 32.4 ppm for V8, 52.1 ppm and 18.9 ppm

for A15). This spectrum shows that a minor fraction of melittin molecules are dynamically disordered in hydrated MBPA-C-melittin-GVA/AAO20, while most molecules are α-helical and have restricted motions.

DISCUSSION

Results described above are significant both from the standpoint of NPC-mimetic sample preparation and from the standpoint of FG-repeat sequence behavior. Regarding sample preparation, our results show that: (i) Phosphonate moieties are readily attached to polypeptide chains through cysteine-maleimide linkages. In experiments described above, the phosphonate moieties were attached to the N-termini of FG30 and melittin peptides, but attachment to the C-termini or other positions are possible; (ii) Spontaneous reaction of phosphonates with aluminum oxide surfaces allows covalent tethering of polypeptides to nanopore walls in AAO. Reaction times on the order of 24 h result in high peptide densities within the nanopores; (iii) In the case of MBPA-C-FG30/AAO20, average peptide concentrations of 90 mM are achievable, corresponding to a 300 mg/ml density that is similar to the density of FG-repeat domains in the central channel of an NPC[24]; (iii) Importantly, covalent tethering to AAO nanopore walls is stable in aqueous solution near pH 7. We observed no changes in NMR spectra of hydrated MBPA-C-FG30-LSAFTG/AAO20 over at least 8 weeks of measurements, with sample temperatures ranging from -5° C to 50° C during these measurements. We also observed no changes in NMR spectra of hydrated MBPA-C-melittin-GVA/AAO20 over at least 5 weeks of measurements; (iv) The high porosity of AAO wafers allows the preparation of samples in which the quantity of nanopore-confined peptide molecules is sufficient for a variety of ^{13}C-detected NMR measurements, including 2D spectroscopy and spin relaxation measurements, with good signal-to-noise ratios for individual ^{13}C-labeled sites.

Measurements on MBPA-C-FG30/AAO20 lead to the following conclusions regarding the behavior of the nanopore-confined FG-repeat peptide: (i) In the hydrated state, ^{13}C and ^{1}H NMR chemical shifts indicate that FG30 has a random-coil conformational distribution at residues distributed over its sequence. The absence of temperature-dependence for chemical shifts of most sites rules out a significant change in conformational preferences from -5° C to 50° C; (ii) Spin relaxation data for all ^{13}C-labeled sites, with the possible exception of T_2^C data for the A16 C_β and T22 C_γ sites, show smooth dependences of relaxation times on temperature. These measurements rule out a phase transition, for example between a state in which tethered FG30 molecules within a nanopore move independently of one another and a state in which groups of molecules move together as a cohesive cluster, since such a transition would produce a discontinuous change in the amplitudes or time scales of molecular motions that drive spin relaxation; (iii) Spin relaxation data indicate multiple modes of molecular motion for tethered FG30 molecules at high concentrations in AAO20 nanopores, including sub-nanosecond motions with restricted amplitudes that drive spin-lattice relaxation and slower, nearly isotropic motions that drive transverse spin relaxation. The weak temperature dependences of T_1^C values indicate that sub-nanosecond motions are not strongly temperature-dependent, while the stronger temperature dependences of T_2^C values indicate that the time scales for nearly isotropic motions decrease by factors of roughly 3-8 from -5° C to 50° C; (iv) In stark contrast to its behavior when tethered in nanopores, MPBA-C-FG30 aggregates to form fibrillar assemblies in free solution at concentrations above 2 mM at 24° C or 40° C (above 5 mM at 4° C), using the same buffer conditions in nanopores or free solution. Thus, tethering to nanopore walls strongly inhibits aggregation of this FG-repeat peptide.

A likely explanation for inhibition of aggregation is that tethering to nanopore walls prevents the close association of neighboring peptide chains required for aggregation. At 90 mM concentration in a 20-nm-diameter pore, the average nearest-neighbor distance between phosphonate groups of tethered MBPA-C-FG30 molecules is approximately 1.9 nm. The length of a fully extended molecule is approximately 10 nm. These numbers imply that contacts between neighboring MBPA-C-FG30 molecules certainly exist within AAO20 nanopores. Therefore, it is conceivable that groups of MBPA-C-FG30 molecules could associate into stable or long-lived oligomeric assemblies within which molecular motions are restricted and conformations are not random-coil-like. Our finding that formation of such assemblies does not occur in MBPA-C-FG30/AAO20 suggests that aggregation of an FG-repeat sequence requires multiple molecules to interact simultaneously through identical sets of intermolecular contacts, similar to the formation of ordered cross-β structures in amyloid fibrils by intrinsically disordered polypeptides[11, 22]. Tethering to nanopore walls may limit the number of molecules that can coalesce into an ordered assembly with sufficient size to be stable.

In the case of hydrated MBPA-C-melittin/AAO20, data in Fig. 10 show that tethering to nanopore walls at high concentrations produces a state in which the majority of peptide chains have restricted motions and α-helical conformations. In free solution near neutral pH and ambient temperatures, melittin is known to form tetrameric, α-helical assemblies in which adjacent melittin helices have an antiparallel alignment[67, 69]. At low pH or elevated temperatures, melittin is random-coil-like and monomeric[68-70]. Since all MBPA-C-melittin molecules in our experiments are tethered to the nanopore walls at their N-termini, antiparallel alignment of neighboring molecules is not possible. Thus, intermolecular interactions in MBPA-C-melittin/AAO20 must be different from intermolecular interactions within a melittin tetramer in free solution. The observation of an α-helical melittin conformation in hydrated MBPA-C-melittin/AAO20 implies that intermolecular contacts promote helix formation by melittin at high concentrations, even when the known tetrameric structure is inaccessible.

Results presented above suggest many directions for future studies. It will be important to apply similar methods to longer FG-repeat sequences, using AAO wafers with larger pore diameters, to test whether nanopore confinement and tethering to nanopore walls has a similar inhibitory effect on aggregation of FG-repeat sequences with lengths closer to those of complete Nup FG-repeat domains. Since the FG-repeat domains within an NPC channel are segments of diverse Nups and therefore have heterogeneous sequences, it is possible that sequence heterogeneity also has an inhibitory effect on aggregation in the true biological context. Simultaneous tethering of heterogeneous FG-repeat sequences within AAO nanopores will therefore be of interest. Effects of post-translational modifications (PTMs) on FG-repeat chain dynamics within AAO nanopores will also be of interest, as PTMs are known to affect NPC function[71-73].

Molecular dynamics simulations of tethered FG-repeat peptides within nanopores, similar to simulations reported by others[10, 74-77], are likely to provide insights into the aggregation inhibition mechanism discussed above, allowing the density of peptide chains, the spacings between their tethering points, and other geometric factors to be varied systematically. Molecular dynamics simulations may also assist with the interpretation and modeling of NMR spin relaxation measurements. Additional spin relaxation measurements will be informative, including ^{15}N relaxation measurements similar to those applied by others in studies of a variety of intrinsically disordered proteins[78].

In addition to FG-repeat domains, the central channels of NPCs contain a high

concentration of NTRs, which may affect the dynamics and the association state of the FG-repeat domains[79]. By including NTRs or segments thereof in the solution used to hydrate the AAO nanopores after tethering the isotopicallylabeled FG-repeat sequences, it may be possible to study the effects of NTRs (or other macromolecules) on the properties of the tethered FG-repeat sequences with NMR measurements. In principle, translational diffusion within FG-repeat-filled nanopores could also be measured with pulsed field-gradient NMR methods[80], allowing dependences of diffusivity on protein sequence, temperature, and other factors to be characterized.

In conclusion, we have introduced an experimental approach for studying properties of polypeptides that are tethered to walls of nanopores with NMR. Measurements on a 30-residue FG-repeat peptide show that tethering within AAO nanopores through phosphonate-surface bonds results in samples that are stable for months or longer, that 90 mM (300 mg/ml) peptide concentrations within nanopores can be achieved, that the conformational and dynamical properties of tethered peptides can be probed with a variety of NMR techniques, and that tethering to nanopore walls strongly inhibits aggregation of the FG-repeat peptide at high concentrations.

ACKNOWLEDGEMENTS

This research was supported by the Intramural Research Program of the National Institute of Diabetes and Digestive and Kidney Diseases (NIDDK) within the National Institutes of Health (NIH). The contributions of the NIH authors are considered Works of the United States Government. The findings and conclusions presented in this paper are those of the authors and do not necessarily reflect the views of the NIH or the U.S. Department of Health and Human Services. We thank Jeff Reece for assistance with confocal fluorescence microscopy, the NIDDK Advanced Light Microscopy and Image Analysis Core for use of its confocal microscope, Dr. Zhuang Wei for assistance with scanning electron microscopy, and the Trans-NIH Shared Resource on Biomedical Engineering and Physical Science for use of its scanning electron microscope. We thank Dr. Ralf G. Nuzzo for suggesting phosphonate/aluminum oxide chemistry as a method for attaching polypeptides within AAO nanopores.

REFERENCES

1. Raices, M.; D'Angelo, M. A., Structure, maintenance, and regulation of nuclear pore complexes: The gatekeepers of the eukaryotic genome. *Cold Spring Harbor Perspect. Biol.* **2022,** *14*, a040691.
2. Grossman, E.; Medalia, O.; Zwerger, M., Functional architecture of the nuclear pore complex. In *Annual Review of Biophysics, Vol 41*, Annual Reviews: Palo Alto, 2012; pp 557-584.
3. Hanover, J. A., The nuclear pore: At the crossroads. *Faseb J.* **1992,** *6*, 2288-2295.
4. Huang, G. X. Y.; Zeng, C.; Shi, Y. G., Structure of the nuclear pore complex goes atomic. *Curr. Opin. Struct. Biol.* **2023,** *78*, 102523.
5. Lin, D. H.; Hoelz, A., The structure of the nuclear pore complex (an update). In *Annual review of biochemistry, vol 88*, Annual Reviews: Palo Alto, 2019; Vol. 88, pp 725-783.
6. Schuller, A. P.; Wojtynek, M.; Mankus, D.; Tatli, M.; Kronenberg-Tenga, R.; Regmi, S. G.; Dip, P. V.; Lytton-Jean, A. K. R.; Brignole, E. J.; Dasso, M.; Weis, K.; Medalia, O.; Schwartz, T. U., The cellular environment shapes the nuclear pore complex architecture. *Nature* **2021,** *598*, 667-671.
7. Zimmerli, C. E.; Allegretti, M.; Rantos, V.; Goetz, S. K.; Obarska-Kosinska, A.; Zagoriy,

I.; Halavatyi, A.; Hummer, G.; Mahamid, J.; Kosinski, J.; Beck, M., Nuclear pores dilate and constrict in cellulo. *Science* **2021,** *374*, eabd9776.
8. Akey, C. W.; Singh, D.; Ouch, C.; Echeverria, I.; Nudelman, I.; Varberg, J. M.; Yu, Z. L.; Fang, F.; Shi, Y.; Wang, J. J.; Salzberg, D.; Song, K. K.; Xu, C.; Gumbart, J. C.; Suslov, S.; Unruh, J.; Jaspersen, S. L.; Chait, B. T.; Sali, A.; Fernandez-Martinez, J.; Ludtke, S. J.; Villa, E.; Rout, M. P., Comprehensive structure and functional adaptations of the yeast nuclear pore complex. *Cell* **2022,** *185*, 361-378.
9. Kato, M.; McKnight, S. L., Cross-β polymerization of low complexity sequence domains. *Cold Spring Harbor Perspect. Biol.* **2017,** *9*, a023598.
10. Raveh, B.; Karp, J. M.; Sparks, S.; Dutta, K.; Rout, M. P.; Sali, A.; Cowburn, D., Slide-and-exchange mechanism for rapid and selective transport through the nuclear pore complex. *Proc. Natl. Acad. Sci. U. S. A.* **2016,** *113*, E2489-E2497.
11. de Opakua, A. I.; Geraets, J. A.; Frieg, B.; Dienemann, C.; Savastano, A.; Rankovic, M.; Cima-Omori, M. S.; Schröder, G. F.; Zweckstetter, M., Molecular interactions of FG nucleoporin repeats at high resolution. *Nat. Chem.* **2022,** *14*, 1278-1285.
12. Najbauer, E. E.; Ng, S. C.; Griesinger, C.; Görlich, D.; Andreas, L. B., Atomic resolution dynamics of cohesive interactions in phase-separated nup98 FG domains. *Nat. Commun.* **2022,** *13*, 1494.
13. Hough, L. E.; Dutta, K.; Sparks, S.; Temel, D. B.; Kamal, A.; Tetenbaum-Novatt, J.; Rout, M. P.; Cowburn, D., The molecular mechanism of nuclear transport revealed by atomic-scale measurements. *eLife* **2015,** *4*, e10027.
14. Milles, S.; Mercadante, D.; Aramburu, I. V.; Jensen, M. R.; Banterle, N.; Koehler, C.; Tyagi, S.; Clarke, J.; Shammas, S. L.; Blackledge, M.; Gräter, F.; Lemke, E. A., Plasticity of an ultrafast interaction between nucleoporins and nuclear transport receptors. *Cell* **2015,** *163*, 734-745.
15. Burke, K. A.; Janke, A. M.; Rhine, C. L.; Fawzi, N. L., Residue-by-residue view of in vitro FUS granules that bind the C-terminal domain of RNA polymerase II. *Mol. Cell* **2015,** *60*, 231-241.
16. Mohanty, P.; Shenoy, J.; Rizuan, A.; Mercado-Ortiz, J. F.; Fawzi, N. L.; Mittal, J., A synergy between site-specific and transient interactions drives the phase separation of a disordered, low-complexity domain. *Proc. Natl. Acad. Sci. U. S. A.* **2023,** *120*, e2305625120.
17. de Opakua, A. I.; Pantoja, C. F.; Cima-Omori, M. S.; Dienemann, C.; Zweckstetter, M., Impact of distinct FG nucleoporin repeats on Nup98 self-association. *Nat. Commun.* **2024,** *15*, 3797.
18. Milles, S.; Bui, K. H.; Koehler, C.; Eltsov, M.; Beck, M.; Lemke, E. A., Facilitated aggregation of FG nucleoporins under molecular crowding conditions. *EMBO Rep.* **2013,** *14*, 178-183.
19. Ng, S. C.; Güttler, T.; Görlich, D., Recapitulation of selective nuclear import and export with a perfectly repeated 12mer GLFG peptide. *Nat. Commun.* **2021,** *12*, 4047.
20. Ader, C.; Frey, S.; Maas, W.; Schmidt, H. B.; Görlich, D.; Baldus, M., Amyloid-like interactions within nucleoporin FG hydrogels. *Proc. Natl. Acad. Sci. U. S. A.* **2010,** *107*, 6281-6285.
21. Molliex, A.; Temirov, J.; Lee, J.; Coughlin, M.; Kanagaraj, A. P.; Kim, H. J.; Mittag, T.; Taylor, J. P., Phase separation by low complexity domains promotes stress granule assembly and drives pathological fibrillization. *Cell* **2015,** *163*, 123-133.
22. Murray, D. T.; Kato, M.; Lin, Y.; Thurber, K. R.; Hung, I.; McKnight, S. L.; Tycko, R.,

Structure of FUS protein fibrils and its relevance to self-assembly and phase separation of low-complexity domains. *Cell* **2017,** *171*, 615-627.
23. Murray, D. T.; Zhou, X. M.; Kato, M.; Xiang, S. H.; Tycko, R.; McKnight, S. L., Structural characterization of the D290V mutation site in hnRNPA2 low-complexity-domain polymers. *Proc. Natl. Acad. Sci. U. S. A.* **2018,** *115*, E9782-E9791.
24. Fragasso, A.; de Vries, H. W.; Andersson, J.; van der Sluis, E. O.; van der Giessen, E.; Dahlin, A.; Onck, P. R.; Dekker, C., A designer FG-Nup that reconstitutes the selective transport barrier of the nuclear pore complex. *Nat. Commun.* **2021,** *12*, 2010.
25. Galvanetto, N.; Ivanovic, M. T.; Grosso, S. A. D.; Chowdhury, A.; Sottini, A.; Nettels, D.; Best, R. B.; Schuler, B., Material properties of biomolecular condensates emerge from nanoscale dynamics. *Proc. Natl. Acad. Sci. U. S. A.* **2025,** *122*, e2424135122.
26. Timney, B. L.; Raveh, B.; Mironska, R.; Trivedi, J. M.; Kim, S. J.; Russel, D.; Wente, S. R.; Sali, A.; Rout, M. P., Simple rules for passive diffusion through the nuclear pore complex. *J. Cell Biol.* **2016,** *215*, 57-76.
27. Kehlenbach, R. H.; Neumann, P.; Ficner, R.; Dickmanns, A., Interaction of nucleoporins with nuclear transport receptors: A structural perspective. *Biol. Chem.* **2023,** *404*, 791-805.
28. Cowburn, D.; Rout, M., Improving the hole picture: Towards a consensus on the mechanism of nuclear transport. *Biochem. Soc. Trans.* **2023,** *51*, 871-886.
29. Stewart, M., Molecular mechanism of the nuclear protein import cycle. *Nat. Rev. Mol. Cell Biol.* **2007,** *8*, 195-208.
30. Hülsmann, B. B.; Labokha, A. A.; Görlich, D., The permeability of reconstituted nuclear pores provides direct evidence for the selective phase model. *Cell* **2012,** *150*, 738-751.
31. Hoogenboom, B. W.; Hough, L. E.; Lemke, E. A.; Lim, R. Y. H.; Onck, P. R.; Zilman, A., Physics of the nuclear pore complex: Theory, modeling and experiment. *Phys. Rep.-Rev. Sec. Phys. Lett.* **2021,** *921*, 1-53.
32. Frey, S.; Görlich, D., FG/FXFG as well as GLFG repeats form a selective permeability barrier with self-healing properties. *Embo J.* **2009,** *28*, 2554-2567.
33. Labokha, A. A.; Gradmann, S.; Frey, S.; Hülsmann, B. B.; Urlaub, H.; Baldus, M.; Görlich, D., Systematic analysis of barrier-forming FG hydrogels from Xenopus nuclear pore complexes. *Embo J.* **2013,** *32*, 204-218.
34. Schmidt, H. B.; Görlich, D., Nup98 FG domains from diverse species spontaneously phase-separate into particles with nuclear pore-like permselectivity. *eLife* **2015,** *4*, e04251.
35. Celetti, G.; Paci, G.; Caria, J.; VanDelinder, V.; Bachand, G.; Lemke, E. A., The liquid state of FG-nucleoporins mimics permeability barrier properties of nuclear pore complexes. *J. Cell Biol.* **2020,** *219*, e201907157.
36. Fisher, P. D. E.; Shen, Q.; Akpinar, B.; Davis, L. K.; Chun, K. K. H.; Baddeley, D.; Saric, A.; Melia, T. J.; Hoogenboom, B. W.; Lin, C. X.; Lusk, C. P., A programmable DNA origami platform for organizing intrinsically disordered nucleoporins within nanopore confinement. *ACS Nano* **2018,** *12*, 1508-1518.
37. Ketterer, P.; Ananth, A. N.; Trip, D. S. L.; Mishra, A.; Bertosin, E.; Ganji, M.; van der Torre, J.; Onck, P.; Dietz, H.; Dekker, C., DNA origami scaffold for studying intrinsically disordered proteins of the nuclear pore complex. *Nat. Commun.* **2018,** *9*, 902.
38. Feng, Q. Z.; Saladin, M.; Wu, C. X.; Cao, E. S.; Zheng, W.; Zhang, A. M. Y.; Bhardwaj, P.; Li, X.; Shen, Q.; Kapinos, L. E.; Kozai, T.; Mariappan, M.; Lusk, C. P.; Xiong, Y.; Lim, R. Y. H.; Lin, C. X., Channel width modulates the permeability of DNA origami-based nuclear pore mimics. *Sci. Adv.* **2024,** *10*, eadq8773.

39. Jovanovic-Talisman, T.; Tetenbaum-Novatt, J.; McKenney, A. S.; Zilman, A.; Peters, R.; Rout, M. P.; Chait, B. T., Artificial nanopores that mimic the transport selectivity of the nuclear pore complex. *Nature* **2009,** *457*, 1023-1027.
40. Ananth, A. N.; Mishra, A.; Frey, S.; Dwarkasing, A.; Versloot, R.; van der Giessen, E.; Görlich, D.; Onck, P.; Dekker, C., Spatial structure of disordered proteins dictates conductance and selectivity in nuclear pore complex mimics. *eLife* **2018,** *7*, e31510.
41. Klughammer, N.; Barth, A.; Dekker, M.; Fragasso, A.; Onck, P. R.; Dekker, C., Diameter dependence of transport through nuclear pore complex mimics studied using optical nanopores. *eLife* **2024,** *12*, RP87174.
42. Kyriakou, N.; Pizzoccaro-Zilamy, M. A.; Nijmeijer, A.; Luiten-Olieman, M.; Winnubst, L., Hydrolytic stability of PEG-grafted γ-alumina membranes: Alkoxysilane vs phosphonic acid linking groups. *Microporous Mesoporous Mat.* **2020,** *307*, 110516.
43. Thissen, P.; Valtiner, M.; Grundmeier, G., Stability of phosphonic acid self-assembled monolayers on amorphous and single-crystalline aluminum oxide surfaces in aqueous solution. *Langmuir* **2010,** *26*, 156-164.
44. Villemin, D.; Moreau, B.; Siméon, F.; Maheut, G.; Fernandez, C.; Montouillout, V.; Caignaert, V.; Jaffrès, P. A., A one step process for grafting organic pendants on alumina via the reaction of alumina and phosphonate under microwave irradiation. *Chem. Commun.* **2001**, 2060-2061.
45. Lee, W.; Park, S. J., Porous anodic aluminum oxide: Anodization and templated synthesis of functional nanostructures. *Chem. Rev.* **2014,** *114*, 7487-7556.
46. Ingham, C. J.; ter Maat, J.; de Vos, W. M., Where bio meets nano: The many uses for nanoporous aluminum oxide in biotechnology. *Biotechnol. Adv.* **2012,** *30*, 1089-1099.
47. Ng, S. C.; Biswas, A.; Huyton, T.; Schünemann, J.; Reber, S.; Görlich, D., Barrier properties of Nup98 FG phases ruled by FG motif identity and inter-FG spacer length. *Nat. Commun.* **2023,** *14*, 747.
48. Yu, M.; Heidari, M.; Mikhaleva, S.; Tan, P. S.; Mingu, S.; Ruan, H.; Reinkemeier, C. D.; Obarska-Kosinska, A.; Siggel, M.; Beck, M.; Hummer, G.; Lemke, E. A., Visualizing the disordered nuclear transport machinery in situ. *Nature* **2023,** *617*, 162-169.
49. Eissler, S.; Kley, M.; Bächle, D.; Loidl, G.; Meier, T.; Samson, D., Substitution determination of FMOC-substituted resins at different wavelengths. *J. Pept. Sci.* **2017,** *23*, 757-762.
50. Thurber, K. R.; Tycko, R., Measurement of sample temperatures under magic-angle spinning from the chemical shift and spin-lattice relaxation rate of ^{79}Br in KBr powder. *J. Magn. Reson.* **2009,** *196*, 84-87.
51. Pines, A.; Gibby, M. G.; Waugh, J. S., Proton-enhanced NMR of dilute spins in solids. *J. Chem. Phys.* **1973,** *59*, 569-590.
52. Morris, G. A.; Freeman, R., Enhancement of nuclear magnetic resonance signals by polarization transfer. *J. Am. Chem. Soc.* **1979,** *101*, 760-762.
53. Bennett, A. E.; Rienstra, C. M.; Auger, M.; Lakshmi, K. V.; Griffin, R. G., Heteronuclear decoupling in rotating solids. *J. Chem. Phys.* **1995,** *103*, 6951-6958.
54. Levitt, M. H.; Freeman, R.; Frenkiel, T., Broad-band heteronuclear decoupling. *J. Magn. Reson.* **1982,** *47*, 328-330.
55. Tycko, R.; Pines, A.; Guckenheimer, J., Fixed-point theory of iterative excitation schemes in NMR. *J. Chem. Phys.* **1985,** *83*, 2775-2802.
56. Takegoshi, K.; Nakamura, S.; Terao, T., ^{13}C-^{1}H dipolar-assisted rotational resonance in

magic-angle spinning NMR. *Chem. Phys. Lett.* **2001,** *344*, 631-637.
57. Braunschweiler, L.; Ernst, R. R., Coherence transfer by isotropic mixing: Application to proton correlation spectroscopy. *J. Magn. Reson.* **1983,** *53*, 521-528.
58. Larimi, M. G.; Tycko, R., Effects of insufficient ^{31}P pulse amplitudes on ^{13}C-detected ^{31}P-^{13}C rotational-echo double-resonance measurements in solid state NMR. *J. Magn. Reson.* **2025,** *377*, 107908.
59. Delaglio, F.; Grzesiek, S.; Vuister, G. W.; Zhu, G.; Pfeifer, J.; Bax, A., Nmrpipe: A multidimensional spectral processing system based on Unix pipes. *J. Biomol. NMR* **1995,** *6*, 277-293.
60. Schindelin, J.; Arganda-Carreras, I.; Frise, E.; Kaynig, V.; Longair, M.; Pietzsch, T.; Preibisch, S.; Rueden, C.; Saalfeld, S.; Schmid, B.; Tinevez, J. Y.; White, D. J.; Hartenstein, V.; Eliceiri, K.; Tomancak, P.; Cardona, A., Fiji: An open-source platform for biological-image analysis. *Nat. Methods* **2012,** *9*, 676-682.
61. Fischer, H.; Polikarpov, I.; Craievich, A. F., Average protein density is a molecular-weight-dependent function. *Protein Sci.* **2004,** *13*, 2825-2828.
62. Wishart, D. S.; Bigam, C. G.; Holm, A.; Hodges, R. S.; Sykes, B. D., ^{1}H, ^{13}C and ^{15}N random coil NMR chemical shifts of the common amino acids. 1. Investigations of nearest-neighbor effects. *J. Biomol. NMR* **1995,** *5*, 67-81.
63. Kjaergaard, M.; Brander, S.; Poulsen, F. M., Random coil chemical shift for intrinsically disordered proteins: Effects of temperature and ph. *J. Biomol. NMR* **2011,** *49*, 139-149.
64. Tycko, R.; Dabbagh, G.; Fleming, R. M.; Haddon, R. C.; Makhija, A. V.; Zahurak, S. M., Molecular dynamics and the phase transition in solid C_{60}. *Phys. Rev. Lett.* **1991,** *67*, 1886-1889.
65. Gunaydin-Sen, O.; Achey, R.; Dalal, N. S.; Stowe, A.; Autrey, T., High resolution ^{15}N NMR of the 225 K phase transition of ammonia borane (NH_3BH_3): Mixed order-disorder and displacive behavior. *J. Phys. Chem. B* **2007,** *111*, 677-681.
66. Becker, E. D., *High resolution NMR: Theory and chemical applications*. 3rd ed.; Academic Press: 2000; p 211.
67. Terwilliger, T. C.; Eisenberg, D., The structure of melittin. 2. Interpretation of the structure. *J. Biol. Chem.* **1982,** *257*, 6016-6022.
68. Wilcox, W.; Eisenberg, D., Thermodynamics of melittin tetramerization determined by circular dichroism and implications for protein folding. *Protein Sci.* **1992,** *1*, 641-653.
69. Jeon, J.; Thurber, K. R.; Ghirlando, R.; Yau, W. M.; Tycko, R., Application of millisecond time-resolved solid state NMR to the kinetics and mechanism of melittin self-assembly. *Proc. Natl. Acad. Sci. U. S. A.* **2019,** *116*, 16717-16722.
70. Wilson, C. B.; Tycko, R., Millisecond time-resolved solid-state NMR initiated by rapid inverse temperature jumps. *J. Am. Chem. Soc.* **2022,** *144*, 9920-9925.
71. Miller, M. W.; Caracciolo, M. R.; Berlin, W. K.; Hanover, J. A., Phosphorylation and glycosylation of nucleoporins. *Arch. Biochem. Biophys.* **1999,** *367*, 51-60.
72. Kosako, H.; Imamoto, N., Phosphorylation of nucleoporins: Signal transduction-mediated regulation of their interaction with nuclear transport receptors. *Nucleus* **2010,** *1*, 309-313.
73. Yoo, T. Y.; Mitchison, T. J., O-GlcNAc modification of nuclear pore complexes accelerates bidirectional transport. *J. Cell Biol.* **2021,** *220*, e202010141.
74. Kreysing, J. P.; Heidari, M.; Zila, V.; Cruz-León, S.; Obarska-Kosinska, A.; Laketa, V.; Rohleder, L.; Welsch, S.; Köfinger, J.; Turonová, B.; Hummer, G.; Kräusslich, H. G.; Beck, M., Passage of the HIV capsid cracks the nuclear pore. *Cell* **2025,** *188*, 930-943.
75. Pulupa, J.; Rachh, M.; Tomasini, M. D.; Mincer, J. S.; Simon, S. M., A coarse-grained

computational model of the nuclear pore complex predicts Phe-Gly nucleoporin dynamics. *J. Gen. Physiol.* **2017,** *149*, 951-966.
76. Moussavi-Baygi, R.; Mofrad, M. R. K., Rapid Brownian motion primes ultrafast reconstruction of intrinsically disordered Phe-Gly repeats inside the nuclear pore complex. *Sci Rep* **2016,** *6*, 299921.
77. Ghavami, A.; van der Giessen, E.; Onck, P. R., Energetics of transport through the nuclear pore complex. *PLoS One* **2016,** *11*, e0148876.
78. Abyzov, A.; Blackledge, M.; Zweckstetter, M., Conformational dynamics of intrinsically disordered proteins regulate biomolecular condensate chemistry. *Chem. Rev.* **2022,** *122*, 6719-6748.
79. Kapinos, L. E.; Huang, B. L.; Rencurel, C.; Lim, R. Y. H., Karyopherins regulate nuclear pore complex barrier and transport function. *J. Cell Biol.* **2017,** *216*, 3609-3624.
80. Roos, M.; Ott, M.; Hofmann, M.; Link, S.; Rössler, E.; Balbach, J.; Krushelnitsky, A.; Saalwächter, K., Coupling and decoupling of rotational and translational diffusion of proteins under crowding conditions. *J. Am. Chem. Soc.* **2016,** *138*, 10365-10372.

Table 1: NMR chemical shifts (ppm relative to DSS) determined from 2D spectra at 20° C of lyophilized MBPA-C-FG30-LSAFTG, dry and hydrated MBPA-C-FG30-LSAFTG/AAO20, and aggregated MBPA-C-FG30-LSAFTG. For hydrated MBPA-C-FG30-LSAFTG/AAO20, both ^{13}C and ^{1}H chemical shifts are given. For other states, only ^{13}C chemical shifts were determined. In lyophilized and dry states, chemical shift values were measured from center-of-mass crosspeak positions. Uncertainties represent FWHM linewidths. "ND" indicates values that could not be determined due to insufficient resolution or crosspeak intensity. In the hydrated and aggregated states, uncertainties are ±0.1 ppm for ^{13}C and ±0.02 ppm for ^{1}H. Random-coil values[62] are given in parentheses along with ^{13}C chemical shifts for the aggregated state.

sample	residue	CO	α	β	γ or aromatic	δ
lyophilized MBPA-C-FG30	L6	175.3±1.5	54.0±1.1	45.8±1.8	27.2±1.3	23.2±1.4
	S11	173.1±1.5	56.7±1.2	66.0±1.8		
	A16	173.9±1.8	49.5±1.5	19.8±2.7		
	F19	ND	55.9±5.0	40.4±3.5	138.7±2.0; 130.6±2.2	
	T22	174.2±2.7	60.6±3.1	69.4±2.1	21.1±2.6	
	G28	173.7±2.6	45.6±2.0			
dry MBPA-C-FG30/AAO20	L6	177.0±2.0	57.2±1.7	41.3±1.6	26.5±1.0	23.3±2.2
	S11	ND	58.7±2.7	63.8±2.2		
	A16	173.9±1.6	49.3±1.5	17.7±3.0		
	F19	ND	56.5±1.5	38.9±1.5	139.3±1.0;130.0±2.0	
	T22	ND	61.0±2.3	68.3±1.7	20.9±2.7	
	G28	173.2±2.8	45.0±1.8			
hydrated MBPA-C-FG30/AAO20	L6	ND	55.1/4.35	42.3/1.54	27.0/1.53	25.0/0.83;23.6/0.79
	S11	ND	58.3/4.48	63.9/3.80		
	A16	ND	50.5/4.48	18.2/1.22		
	F19	ND	57.9/4.52	39.6/3.00	131.6/7.17;129.9/7.17	
	T22	ND	61.7/4.37	69.7/4.19	21.61/1.12	
	G28	ND	45.4/3.81			
aggregated MBPA-C-FG30/AAO20	L6	176.8 (177.6)	54.4 (55.1)	45.4 (42.4)	29.1 (26.9)	26.4 (24.9,23.3)
	S11	172.6 (174.6)	60.4 (58.3)	64.6 (63.8)		
	A16	171.8 (175.9)	50.0 (50.5)	19.0 (18.1)		
	F19	178.1 (175.8)	57.0 (57.7)	41.7 (39.6)	ND	
	T22	174.2 (174.7)	63.3 (61.8)	70.0 (69.8)	22.5 (21.5)	
	G28	174.4 (174.9)	47.0 (45.1)			

Table 2: Loading of MBPA-C-FG30 in AAO20 produced by various incubation conditions, as determined from signal areas in 1D ^{13}C and ^{31}P NMR spectra. Uncertainties were calculated from the RMS noise in the spectra.

sample number	labeled residues in MBPA-C-FG30	incubation time	dry mass in MAS rotor (mg)	type of NMR spectrum	total FG30 loading (μmol)	FG30 loading per milligram of AAO20 (nmol)
1	G2, G10, G20, G29	24 h	16.9	^{13}C CP	0.125 ± 0.003	7.39 ± 0.20
1	G2, G10, G20, G29	24 h	16.9	^{31}P CP	0.082 ± 0.005	4.85 ± 0.30
2[a]	G2, G10, G20, G29	24 h	28.8	^{13}C CP	0.131 ± 0.002	4.57 ± 0.07
2[a]	G2, G10, G20, G29	24 h	28.8	^{13}C DP	0.145 ± 0.007	5.02 ± 0.25
2[a,b]	G2, G10, G20, G29	24 h	28.8	^{13}C DP	0.097 ± 0.003	3.38 ± 0.09
2[a,b]	G2, G10, G20, G29	24 h	28.8	^{31}P CP	0.098 ± 0.011	3.41 ± 0.39
3[c]	G2, G10, G20, G29	24 h	15.9	^{13}C CP	0.057 ± 0.001	3.57 ± 0.08
4[b,d]	G2, G10, G20, G29	24 h	4.9	^{13}C CP	0.025 ± 0.002	5.13 ± 0.33
5	G2, G10, G20, G29	41 h	15.0	^{13}C CP	0.105 ± 0.002	7.01 ± 0.18
5	G2, G10, G20, G29	41 h	15.0	^{13}C DP	0.080 ± 0.007	5.35 ± 0.44
6[a]	G2, G10, G20, G29	64 h	28.6	^{13}C CP	0.124 ± 0.004	4.34 ± 0.14
6[a]	G2, G10, G20, G29	64 h	28.6	^{13}C DP	0.134 ± 0.013	4.70 ± 0.46
6[a]	G2, G10, G20, G29	64 h	28.6	^{31}P CP	0.152 ± 0.009	5.32 ± 0.33
7[a,e]	G2, G10, G20, G29	64 h	29.0	^{13}C CP	0.128 ± 0.004	4.42 ± 0.14
7[a,e]	G2, G10, G20, G29	64 h	29.0	^{13}C DP	0.118 ± 0.010	4.05 ± 0.34
8	L6, S11, A16, F19, T22, G28	65 h	15.1	^{13}C CP	0.095 ± 0.003	6.27 ± 0.20
8	L6, S11, A16, F19, T22, G28	65 h	15.1	^{13}C DP	0.091 ± 0.004	6.01 ± 0.24
8	L6, S11, A16, F19, T22, G28	65 h	15.1	^{31}P CP	0.099 ± 0.008	6.53 ± 0.53
8[b]	L6, S11, A16, F19, T22, G28	65 h	15.1	^{13}C DP	0.089 ± 0.002	5.88 ± 0.12
9[f]	G2, G10, G20, G29	66 h	16.0	^{13}C CP	0.094 ± 0.002	5.90 ± 0.14
9[f]	G2, G10, G20, G29	66 h	16.0	^{13}C DP	0.109 ± 0.009	6.82 ± 0.58
9[f]	G2, G10, G20, G29	66 h	16.0	^{31}P CP	0.077 ± 0.005	4.80 ± 0.34
10	G2, G10, G20, G29	96 h	7.6	^{13}C CP	0.037 ± 0.001	4.86 ± 0.14
10	G2, G10, G20, G29	96 h	7.6	^{31}P CP	0.034 ± 0.008	4.42 ± 1.00
11	L6, S11, A16, F19, T22, G28	185 h	14.4	^{13}C CP	0.090 ± 0.002	6.26 ± 0.17
11	L6, S11, A16, F19, T22, G28	185 h	14.4	^{13}C DP	0.093 ± 0.002	6.45 ± 0.14
11	L6, S11, A16, F19, T22, G28	185 h	14.4	^{31}P CP	0.080 ± 0.003	5.54 ± 0.24
11[b]	L6, S11, A16, F19, T22, G28	185 h	14.4	^{13}C DP	0.081 ± 0.002	5.63 ± 0.15
11[b]	L6, S11, A16, F19, T22, G28	185 h	14.4	^{31}P CP	0.097 ± 0.014	6.75 ± 1.00
12	L6, S11, A16, F19, T22, G28	24 h	46.6	^{13}C CP	0.266 ± 0.003	5.71 ± 0.07
12	L6, S11, A16, F19, T22, G28	24 h	46.6	^{13}C DP	0.273 ± 0.005	5.87 ± 0.11

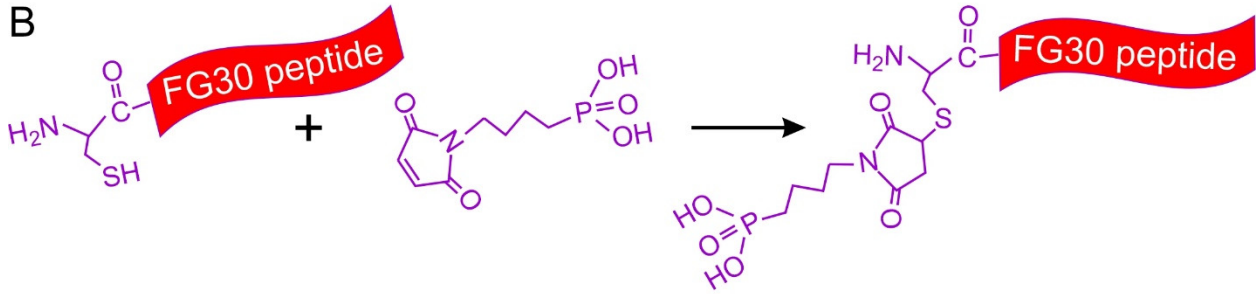
12	L6, S11, A16, F19, T22, G28	24 h	46.6	^{31}P CP	0.265 ± 0.006	5.68 ± 0.14

[a] Three AA20 wafers incubated in one tube containing 1.0 ml of 1.0 mM MBPA-C-FG30, rather than 1.00 ml of 1.0 mM MBPA-C-FG30 per wafer in separate tubes.
[b]NMR measurements performed on hydrated MBPA-C-FG30/AAO20, rather than dry MBPA-C-FG30/AAO20.
[c]AAO with 40 nm pores (AAO40) used instead of AAO20.
[d]AAO20 with 5 µm thickness, rather than 50 µm.
[e]AAO20 wafers were crushed into pieces with diameters of approximately 2 mm before incubation.
[f]1.0 mM MBPA-C-FG30 in 25 mM acetate buffer, pH 5.6, rather than 0.2 M Bis-Tris buffer, pH 6.5.

A

```
AGTTTGLFGS SPATSSATGL FSSSTTNSGF AYGQNKTAFG TSTTGFGTNP
GGLFGQQNQQ TTSLFSKPFG QATTTQNTGF SFGNTSTIGQ PSTNTMGLFG
VTQASQPGGL FGTATNTSTG TAFGTGTGLF GQTNTGFGAV GSTLFGNNKL
TTFGSSTTSA PSFGTTSGGL FGNKPTLTLG TNTNTSNFGF GTNTSGNSIF
GSKPAPGTLG TGLGAGFGTA LGAGQASLFG NNQPKIGGPL GTGAFGAPGF
NTTTATLGFG APQAPVALTD PNASAAQQAV LQQHINSLTY SPFGDSPLFR
```

B



C

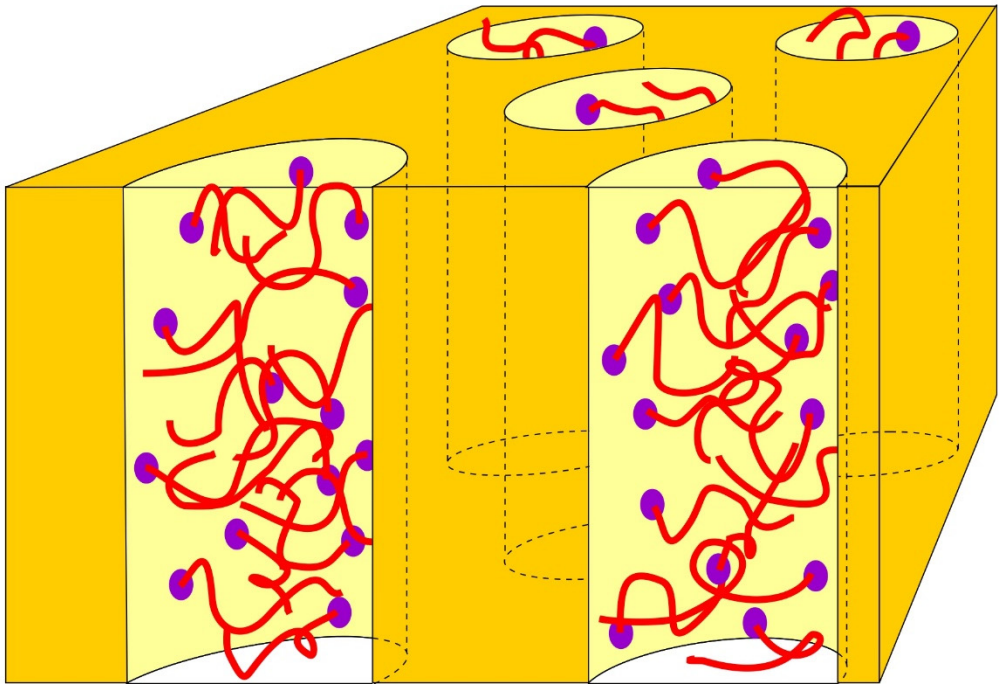


Figure 1: (A) Sequence of the second FG-repeat domain of human Nup98 (Uniprot code P52948, residues 221-520). FG dyads are highlighted in yellow. The FG30 segment studied in this work is shown in red. (B) Method for introducing a phosphonate group by conjugating 4-maleimidobutylphosphonic acid to an N-terminal cysteine to produce MBPA-C-FG30. (C) Cartoon representation of peptides tethered to the walls of nanopores in AAO by reaction of phosphonate groups with aluminum oxide surfaces.

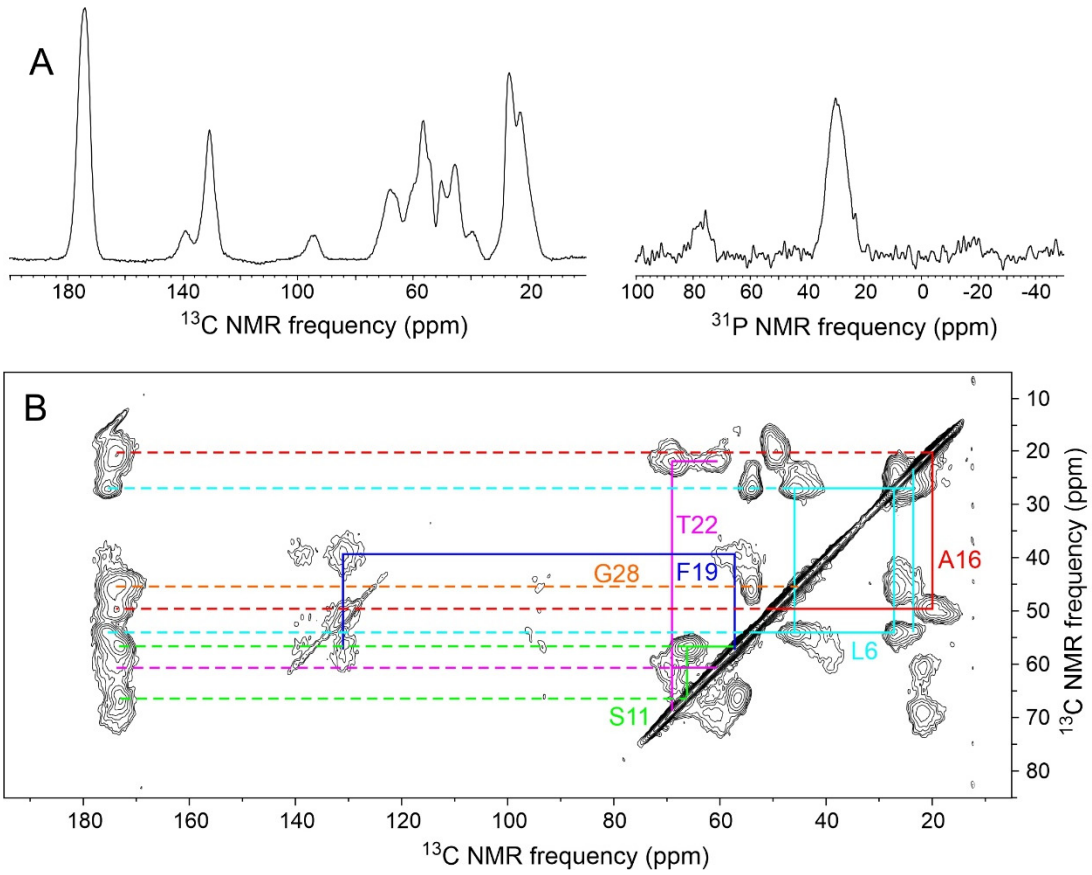


Figure 2: (A) 1D ^{13}C and ^{31}P spectra of lyophilized MBPA-C-FG30-LSAFTG, recorded in a 14.1 T field at 20° C with ^{1}H-^{13}C cross-polarization, high-power ^{1}H decoupling, and MAS at 12.00 kHz. The sample mass was 6.0 mg, and spectra were obtained with 512 scans and 1024 scans, respectively. (B) 2D ^{13}C-^{13}C spectrum of the same sample, recorded with a 30 ms DARR mixing period, a maximum t_1 value of 3.175 ms, and a total of 65536 scans. Color-coded lines indicate assignments of crosspeaks to the six ^{15}N,^{13}C-labeled residues. Contour levels increase by successive factors of 1.5.

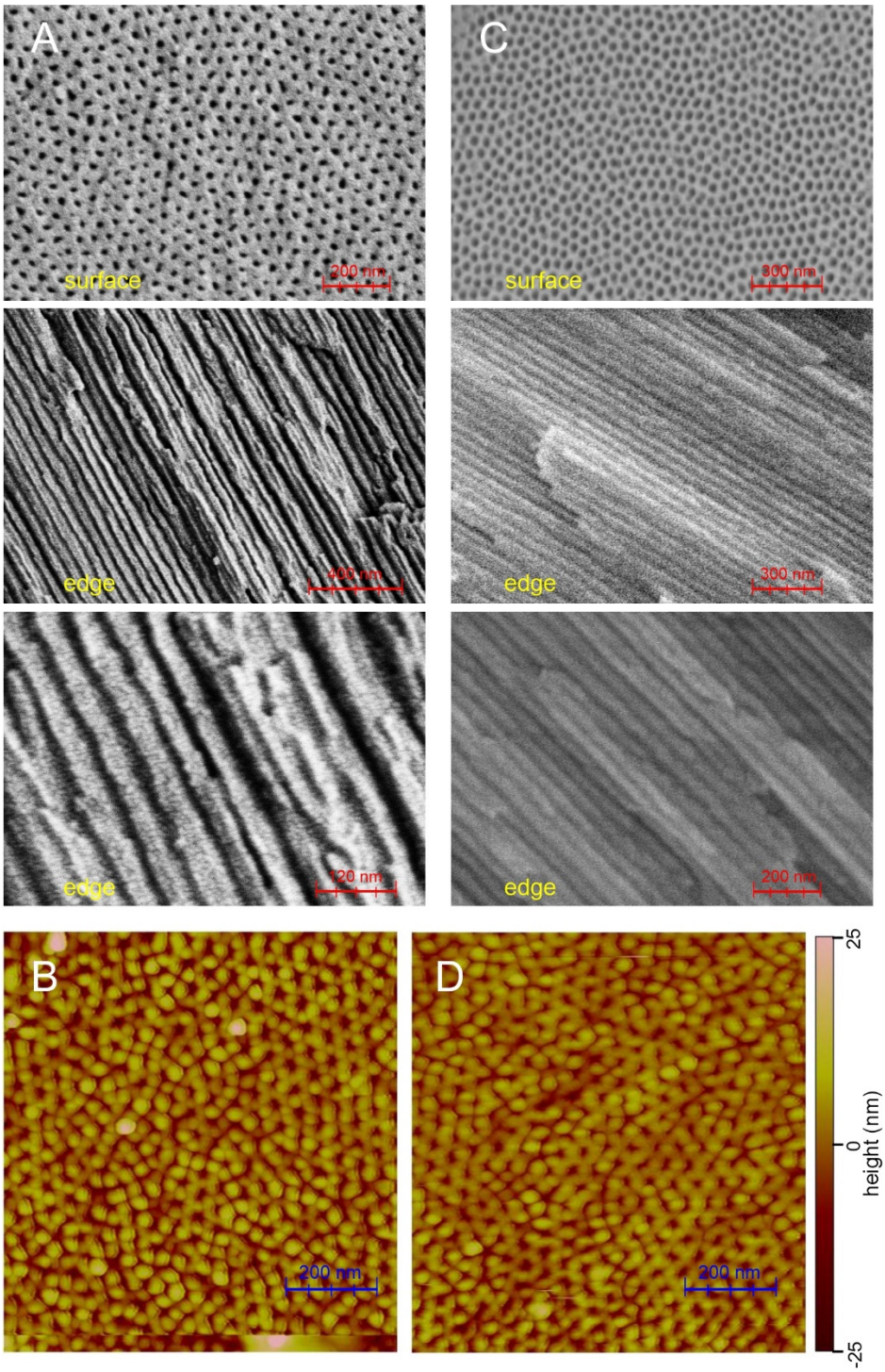


Figure 3: (A) SEM images of an untreated AAO20 wafer. Upper image shows the wafer surface. Images below show edges that were exposed after breaking the wafer. (B) AFM image of the surface of an untreated AAO20 wafer. (C) SEM images of an AAO20 wafer after treatment with 0.1 M H_2SO_4 to remove surface phosphate, followed by incubation with 1.0 mM MBPA-C-FG30 in 0.2 M Bis-Tris buffer, pH 6.5, at 40° C for 24 h. (D) AFM image after treatment with 0.1 M H_2SO_4 (6 min treatment followed by H_2O rinses, repeated twice as described in the text).

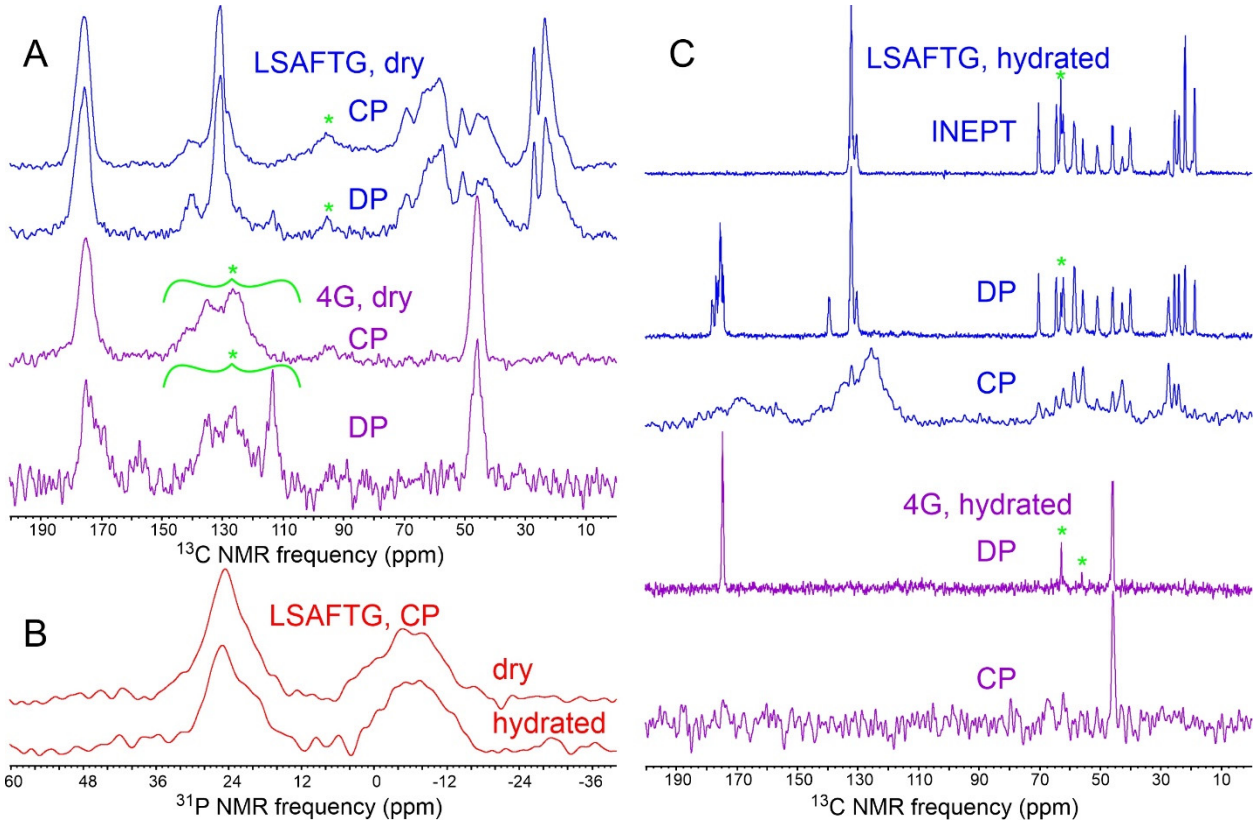


Figure 4: (A) 1D ^{13}C NMR spectra of MBPA-C-FG30-LSAFTG/AAO20 and MBPA-C-FG30-4G/AAO20 in dry states after thorough rinsing with H_2O, obtained with ^{1}H-^{13}C cross-polarization or with direct pulsing. Samples contained 45.7 mg of AAO20 and 0.27 µmol of MBPA-C-FG30-LSAFTG or 28.3 mg of AAO20 and 0.14 µmol of MBPA-C-FG30-4G (samples 12 and 2 in Table 2, respectively). Green asterisks indicate MAS sideband signals and probe background signals. (B) Cross-polarized 1D ^{31}P NMR of the MBPA-C-FG30-LSAFTG/AAO20 sample in dry and hydrated states. Both spectra were acquired at 20° C with 5120 scans. Signals centered at 24 ppm and -6 ppm arise from MBPA-C-FG30 phosphonate groups and residual surface phosphate groups, respectively. (C) 1D ^{13}C NMR spectra of the samples in panel A after hydration with 0.2 M Bis-Tris buffer, pH 6.5, obtained with cross-polarization, direct pulsing, or ^{1}H-^{13}C INEPT. Green asterisks indicate natural-abundance ^{13}C signals from the Bis-Tris buffer. All spectra in panels A and C were acquired at 20° C with 2048 scans.

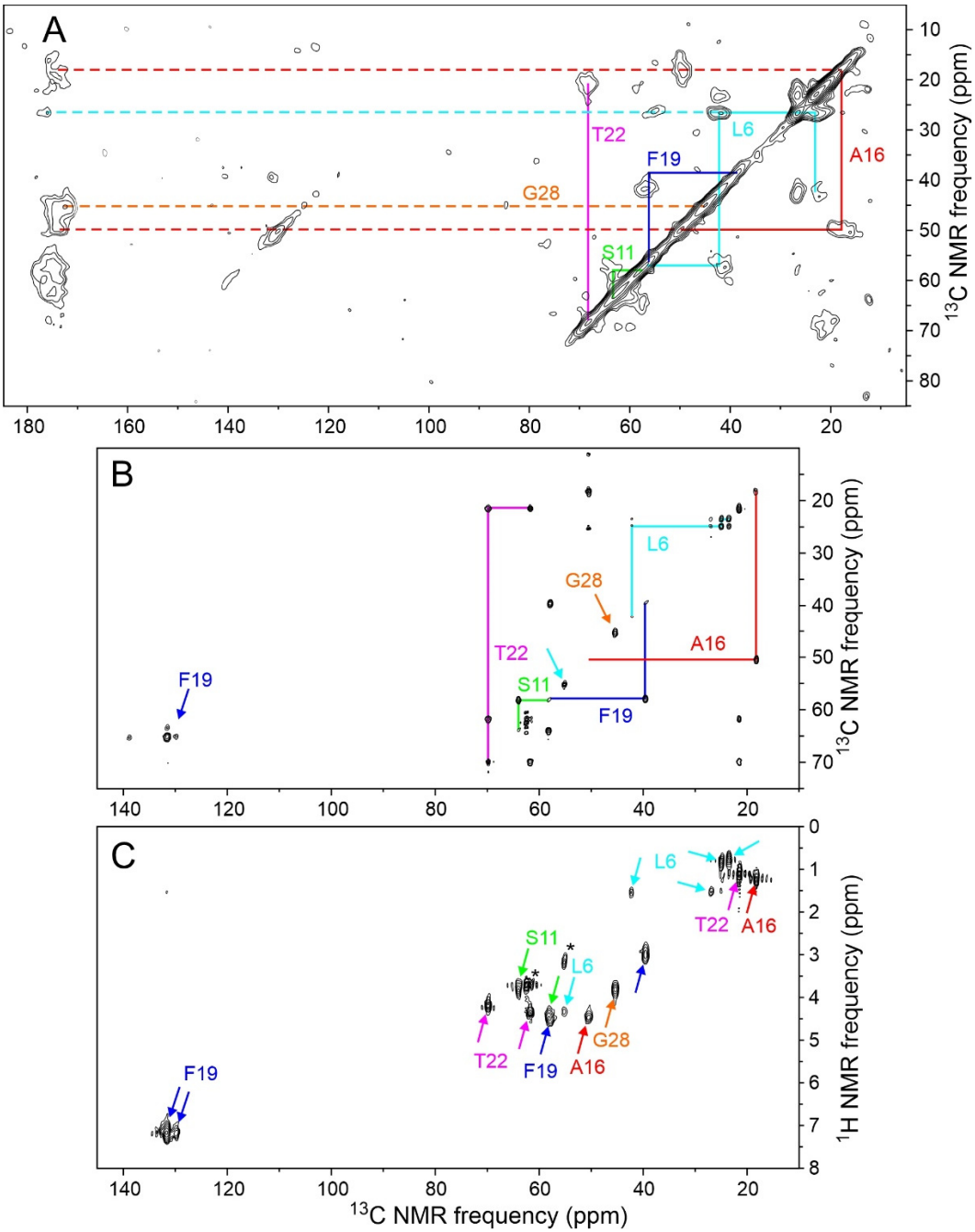


Figure 5: (A) 2D ^{13}C-^{13}C NMR spectrum of dry MBPA-C-FG30-LSAFTG/AAO20 (same sample as in Fig. 4A), obtained with a 30 ms DARR mixing period. Measurement conditions were the same as in Fig. 2B, except that the total number of scans was 32768. Contour levels increase by successive factors of 1.5. (B) 2D ^{13}C-^{13}C NMR spectrum of hydrated MBPA-C-FG30-LSAFTG/AAO20 (same sample as in Fig. 4C), obtained with ^{1}H-^{13}C INEPT and a 12.5 ms isotropic ^{13}C-^{13}C mixing period. (C) 2D ^{1}H-^{13}C NMR spectrum of hydrated MBPA-C-FG30-LSAFTG/AAO20, obtained with INEPT polarization transfers. Asterisks indicate natural-abundance crosspeaks from the Bis-Tris buffer. Contour levels in panels B and C increase by successive factors of 1.8. All spectra were acquired at 20° C.

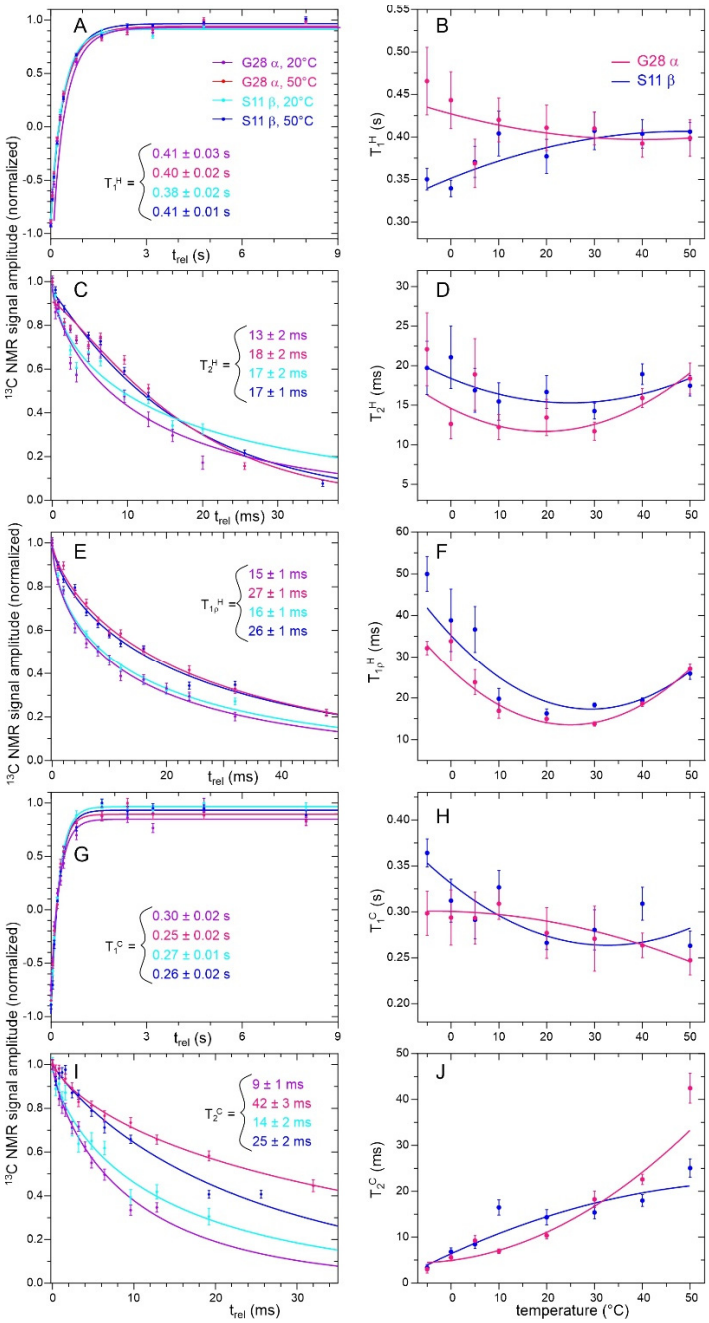


Figure 6: Examples of measurements of nuclear spin relaxation times for hydrated MBPA-C-FG30-LSAFTG/AAO20 (same sample as in Fig. 5B). (A,C,E,G,I) Measurements of ^{13}C-detected T_1^H, ^{13}C-detected T_2^H, ^{13}C-detected $T_{1\rho}^H$, T_1^C, and T_2^C values for the S11 C_β and G28 C_α sites at 20° C and 50° C. Solid lines in are stretched-exponential fits in panels A, C, E, and I, and single-exponential fits in panel G, yielding the indicated relaxation times. Error bars represent uncertainties derived from the RMS noise in the ^{13}C NMR spectra. (B,D,F,H,J) Temperature dependences of the spin relaxation times. Solid lines are second-order polynomial fits, intended to serve as guides to the eye. Error bars represent standard errors in the fitted relaxation time values.

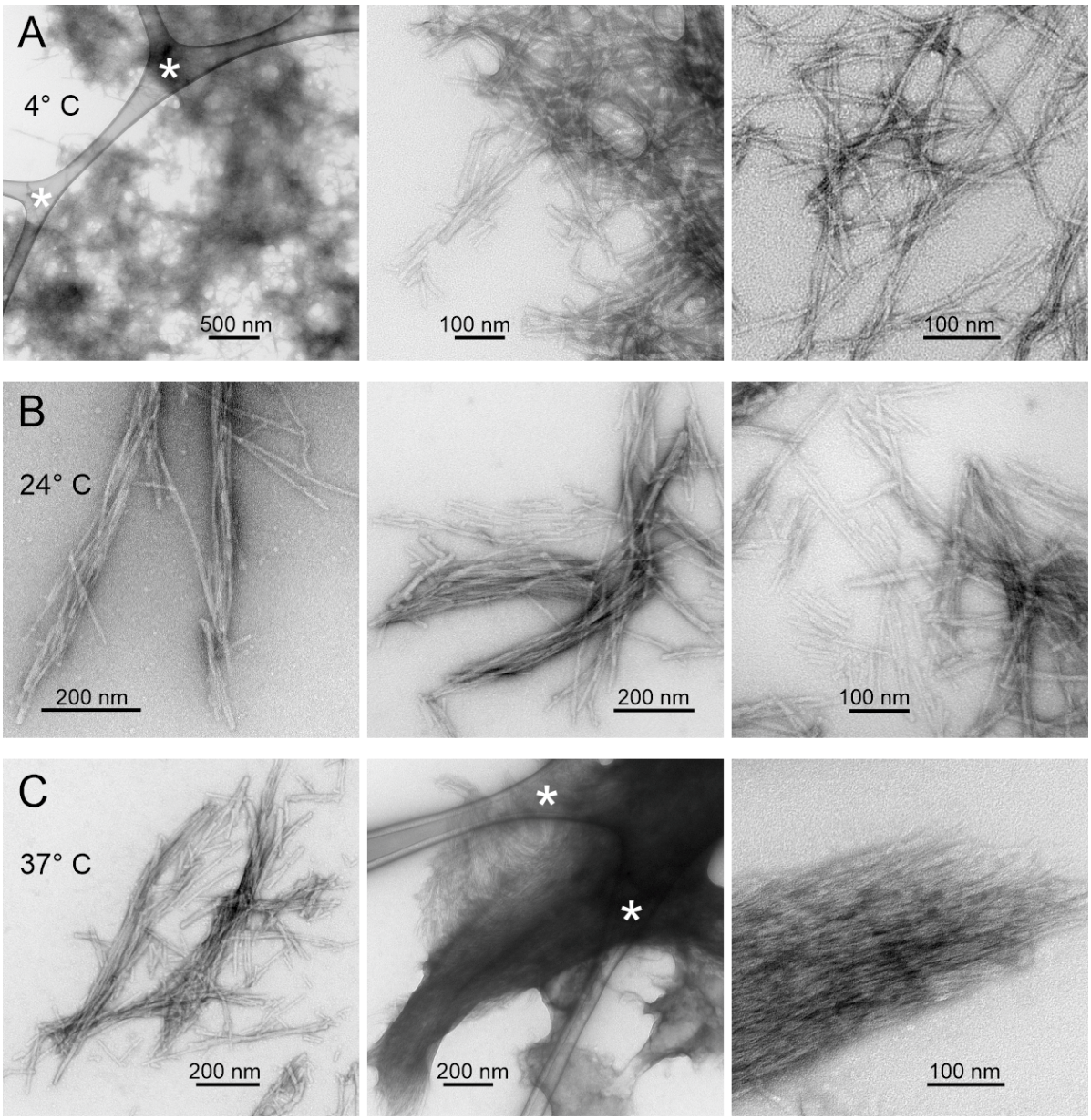


Figure 7: TEM images of aggregated MBPA-C-FG30, negatively stained with uranyl acetate. Aggregated material developed spontaneously at 10 mM peptide concentration in 0.2 M Bis-Tris buffer, pH 6.5, during incubation at 4° C (A), 24° C (B), or 37° C (C). Asterisks indicate features from the carbon lace that supports the thin carbon films to which aggregated MBPA-C-FG30 is adsorbed on the TEM grids.

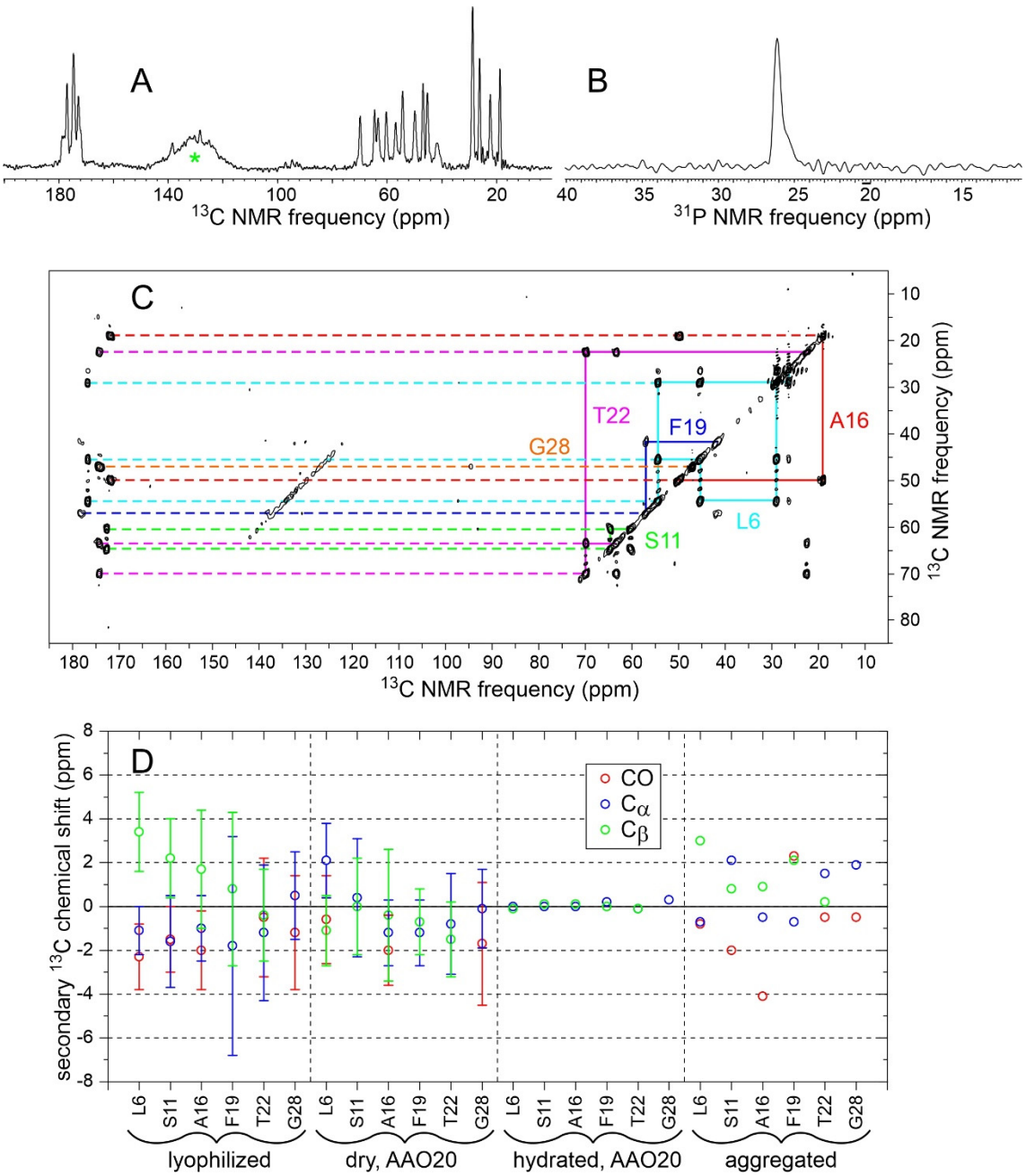


Figure 8: (A,B) Cross-polarized 1D ^{13}C NMR and directly-pulsed 1D ^{31}P spectra of aggregated MBPA-C-FG30-LSAFTG in a fully hydrated state. Green asterisk in panel A indicates a probe background signal. (C) 2D ^{13}C-^{13}C NMR spectrum of the same sample, obtained with ^{1}H-^{13}C cross-polarization and a 30 ms DARR mixing period. Measurement conditions were the same as in Fig. 5A. Contour levels increase by successive factors of 1.8. All spectra were recorded at 20° C. (D) Secondary ^{13}C chemical shifts for backbone CO, C_α, and C_β sites determined from 2D ^{13}C-^{13}C NMR spectra of MBPA-C-FG30-LSAFTG in lyophilized, dry AAO20-bound, hydrated AAO20-bound, and aggregated states (Figs. 2B, 5A, 5B, and 8C). Error bars for lyophilized and dry AAO20 bound states represent FWHM ^{13}C linewidths, determined from 1D slices through crosspeaks in the 2D spectra.

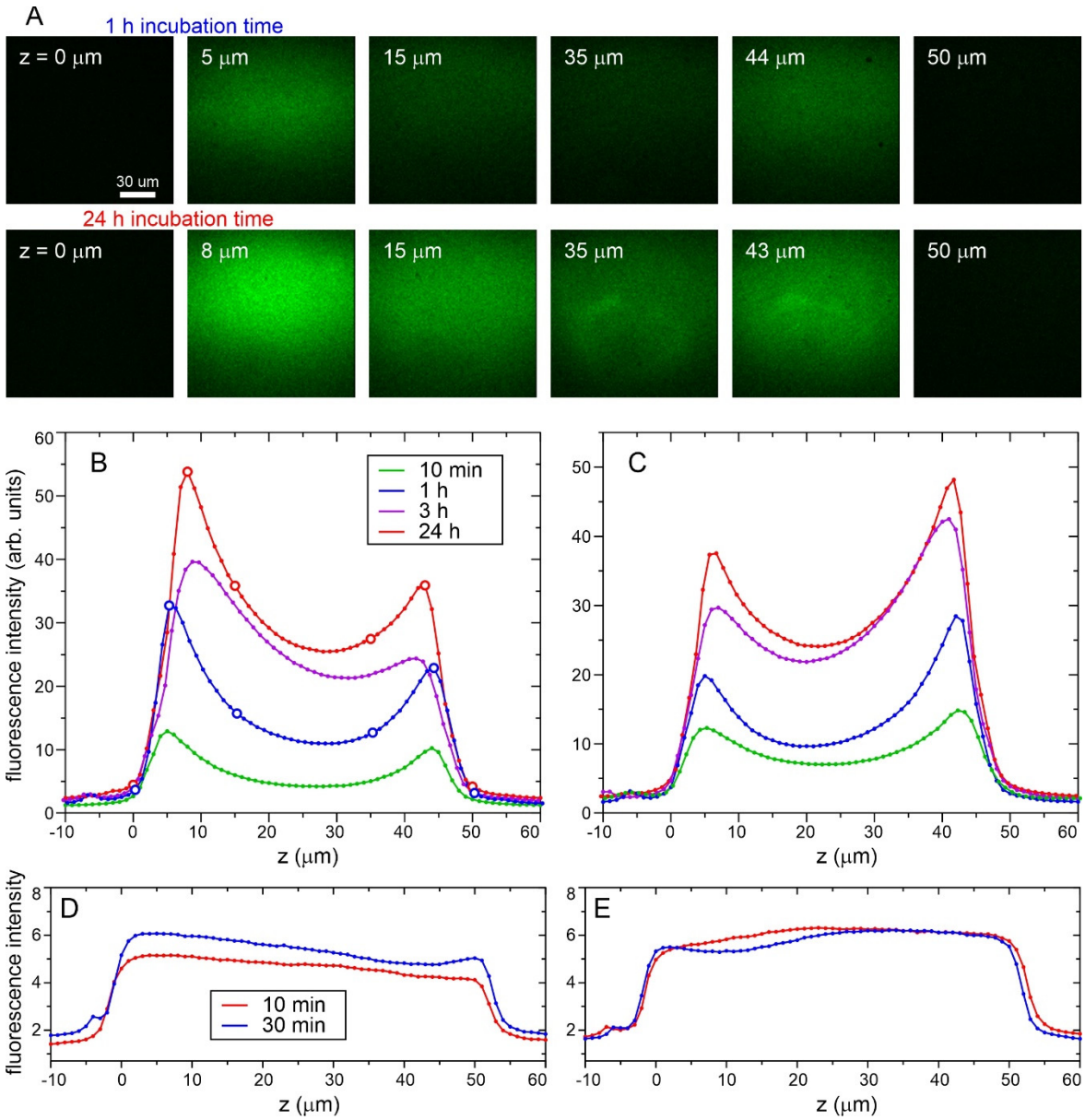


Figure 9: (A) Confocal fluorescence microscope images of AAO20 wafers after incubation at 40° C for 1 h or 24 h in 1.0 mM FITC-labeled MBPA-C-FG30 (2.5% labeling). Fluorescence was excited at 405 nm and collected at 514–585 nm. Images are shown for indicated distances z into the wafer, with z = 0 μm defined as a position of the confocal point slightly outside the wafer. (B) Dependence of fluorescence intensity on z for samples with the indicated incubation times, obtained by averaging the intensity within images at increasing z values. Open circles are the positions shown in panel A. (C) Fluorescence intensity profiles after flipping each sample in panel B, so that excitation light enters and fluorescence is detected from the opposite side of the wafer. (D) Fluorescence intensity profiles for AAO20 wafers that were incubated at 24° C in solutions containing 50 μg/ml fluorescein and 6 M GuHCl for 10 min or 30 min. (E) Fluorescence intensity profiles after flipping the samples in panel D.

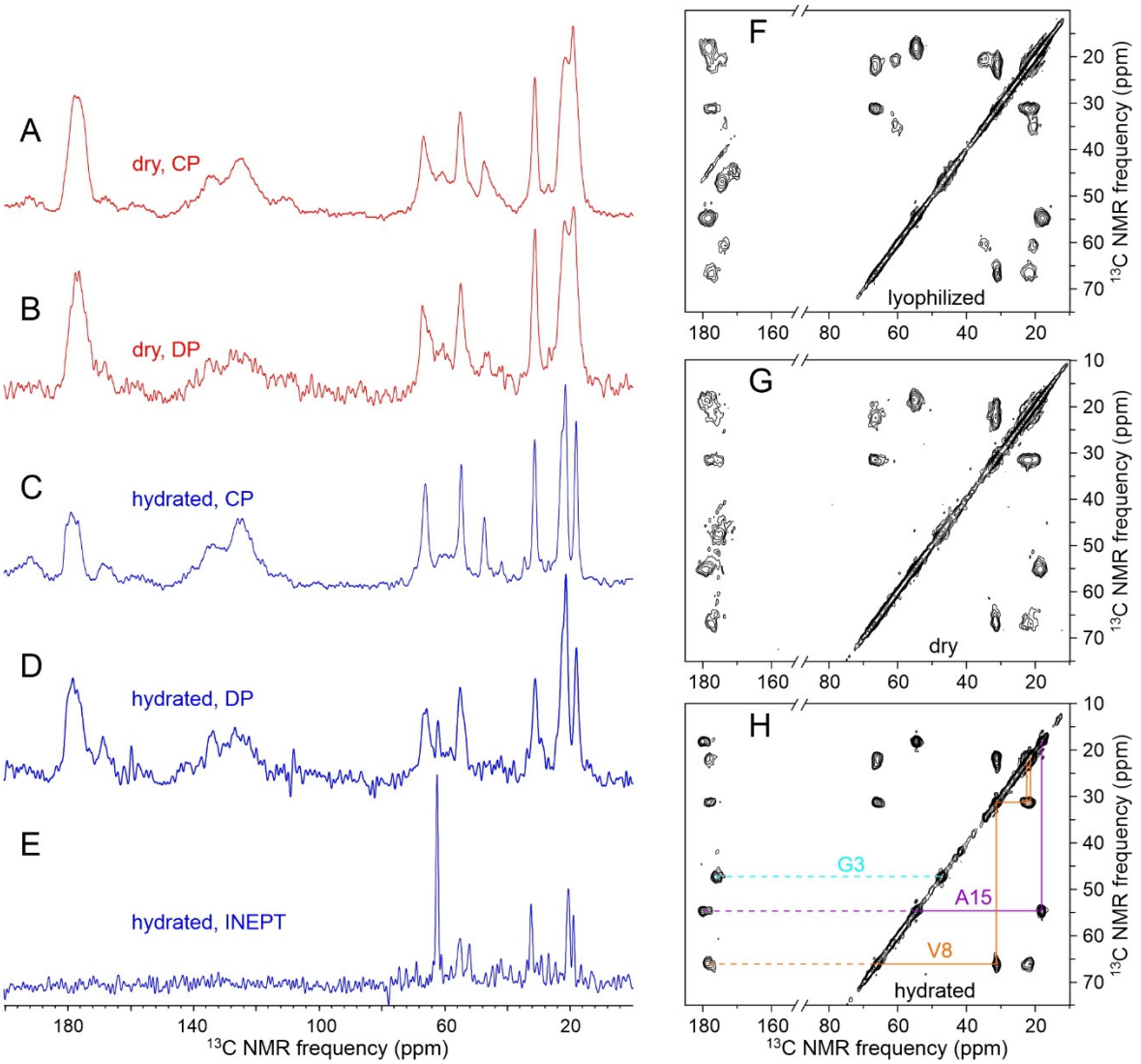


Figure 10: (A,B) 1D ^{13}C NMR spectra of dry MBPA-C-melittin-GVA/AAO20, recorded with ^{1}H-^{13}C cross-polarization or direct pulsing and with 1024 scans. Total sample mass was 48.9 mg, including 0.40 ± 0.03 μmole of MBPA-C-melittin-GVA. (C,D) 1D ^{13}C NMR spectra of MBPA-C-melittin-GVA/AAO20 after hydration with 50 mM Bis-Tris, pH 6.5, recorded with ^{1}H-^{13}C cross-polarization or direct pulsing and with 1024 scans. (E) 1D ^{13}C NMR spectrum of the hydrated sample, recorded with ^{1}H-^{13}C INEPT, low-power ^{1}H decoupling, and 32768 scans. Aliphatic signal areas per scan in panels A-E have ratios of 100.0:36.9:59.8:26.2:2.5. Approximately 30% of the dry sample was lost in the hydration process. (F,G,H) 2D ^{13}C-^{13}C NMR spectra of a 1.4 mg sample of lyophilized MPBA-C-melittin-GVA powder, the dry MBPA-C-melittin-GVA/AAO20 sample, and the hydrated MBPA-C-melittin-GVA/AAO20 sample. All 2D spectra used 30 ms DARR mixing, a maximum t_1 value of 3.180 ms, and a total of 122880 scans. Contour levels in 2D spectra increase by successive factors of 1.5. All spectra were recorded at 17.5 T and 32° C, with MAS at 12.5 kHz. Gaussian line broadening of 100 Hz was applied in all 1D spectra (except panel E, which used 50 Hz) and in both dimensions of the 2D spectra.