Mobile Eye-Tracking Glasses Capture
Ocular and Head Markers of Listening Effort

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Abstract: To extend the assessment of listening effort beyond a sound booth, we validated mobile eye-tracking glasses (Pupil Labs Neon) by comparing them to a stationary system (Eyelink DUO) in a controlled environment. We recorded eye movements, pupil size, and head movements from 26 young adults during a speech-in-noise task. When listening conditions became challenging, we observed reduced gaze dispersion and increased pupil sizes of similar magnitude from both devices, in addition to reduced head movements recorded solely by the mobile device. These findings suggest that mobile eye-trackers reliably capture listening effort, paving the path towards assessments in daily settings.

Keywords: listening effort, mobile eye-tracking glasses, pupillometry, eye movements, head movements

1. Introduction

Comprehending speech in noisy environments, such as a crowded restaurant, places high cognitive demand on attentional and memory resources, requiring listening effort (Herrmann & Johnsrude, 2020; Peelle, 2018; Pichora-Fuller et al., 2016a). Such effort is often considered an early indicator of hearing loss, making its objective assessment critical for clinical and research purposes (Helfer & Jesse, 2021; Herrmann & Johnsrude, 2020; Pichora-Fuller et al., 2016). To date, pupillometry is one of the most commonly used objective markers to listening effort, with numerous studies demonstrating that pupil size increases as listening becomes more demanding (Almaraz et al., 2018; Piquado et al., 2010; Van Der Wel & Van Steenbergen, 2018; Winn et al., 2018a; Zekveld et al., 2018). More recently, a separate line of work indicates that a reduction in eye movements may also index listening effort, potentially through pupil-independent mechanisms (Cui & Herrmann, 2023; Herrmann & Ryan, 2024). Assessing listening effort using eye movements offers a distinct advantage compared to pupillometry: eye-based metrics are less sensitive to environmental factors like ambient lighting, stimulus luminance, and baseline physiological fluctuations (Fink et al., 2024; Thurman et al., 2021; Winn et al., 2018a; Zekveld et al., 2018). This makes eye movements a promising candidate for assessing listening effort in more natural, real-world situations. However, both pupillometry and eye-movement research have mainly relied on stationary eye-trackers that require restricted head movements, limiting the ecological validity of these assessments.

Modern mobile eye-tracking glasses present an opportunity to overcome these limitations and move assessments towards real-world, out-of-lab contexts. These portable devices have been successfully used to track eye movements and pupil size across different age groups and hearing abilities (Chavant & Kapoula, 2022; Hidalgo et al., 2023; Perea Perez, 2023) for various auditory tasks, such as music listening and performing (Saxena et al., 2025; Vandemoortele et al., 2018), sound localization (Alemu et al., 2024), and speech-in-noise perception (Perea Perez, 2023). This evidence suggests that mobile eye-trackers could effectively measure listening effort. For example, promising correspondence between mobile eye-tracking glasses and a stationary EyeLink eye-tracker (the most commonly used system to achieve high temporal

48 and spatial precision) has been found for simple oculomotor tasks (Ehinger et al., 2019). However, it

49 remains unclear whether relative measures, such as gaze dispersion (Cui & Herrmann, 2023; Herrmann et

50 al., 2025; Herrmann & Ryan, 2024), a sensitive metric capturing changes in eye movements is robust

51 enough to concurrent reduction in both spatial and temporal resolution.

52  Beyond expanding previously established listening effort measures from stationary to mobile devices,

mobile eye-trackers provide additional unique metrics that may be relevant to listening effort. For instance,

head movements (e.g., measured via inertial motion units embedded in head-mounted eye-trackers) may

index cognitive load in a manner like eye movements, however, this has not been examined. Listeners

reduce eye movements during difficult listening, possibly to limit distracting visual input (Cui & Herrmann,

2023). A similar pattern might occur to head movements, where a reduction in head movements might

reduce distracting somatosensory inputs, in turn freeing up cognitive resources for a listening task (Higgins

et al., 2023). Integrating these markers could provide a comprehensive and ecologically valid approach to

monitoring the dynamics of listening effort through mobile glasses.

61  The present study examines whether modern mobile eye-tracking glasses (Pupil Labs' Neon) are

similarly sensitive to pupil-size and eye-movement markers of listening effort as a stationary eye-tracking

system (EyeLink Duo). We also investigate whether head movements index listening effort. To this end,

we concurrently measured pupil size, gaze dispersion, and head-movement variability with synchronized

stationary and mobile devices concurrently while younger, normal-hearing adults performed a speech-

comprehension task under easy and difficult speech-masking conditions.

2. Methods

2.1 Participants

69  Twenty-six younger adults (M = 25.75 years, SD = 5.25, range = 18-35 years; 17 females, 6 males, 1

agender, 2 non-binary) participated in the study. All self-reported being native English speakers, having

normal vision and hearing, and having no severe psychological or neurological conditions. All participants

provided written informed consent and received $20 per hour for their participation. Two additional

individuals participated, but their data were not recorded (N=1) or the data timestamp procedure failed

(N=1). The study was approved by the Research Ethics Board at Baycrest Academy for Research and

Education.

2.2 Experiment Setup and Procedure

Participants sat in a sound-attenuating booth with their head stabilized on a chin and forehead rest,

positioned approximately 70 cm from a computer monitor. Auditory stimuli were presented binaurally

through Sony MDR-7506 headphones, with sound played through a Steinberg UR22 mkII external sound

card. The experiment was programmed in MATLAB using Psychtoolbox (v3.0.14). The main task was a

speech-in-noise perception task. Participants listened to 180 Harvard sentences (mean duration = 2.5 s;

Institute of Electrical and Electronics Engineers, 1969) presented in a 7-s 12-talker babble noise (Bilger,

1984), either under an easy (+11 dB SNR) or difficult (-4 dB SNR) listening condition. The sentence

started 1.5-s after babble onset and the SNR was determined by adjusting the level of the speech, whereas

the level of the babble was constant across trials (Kadem et al., 2020; Ohlenforst et al., 2017). The

computer screen remained blank before and during sound presentation. After each sentence, a probe word

appeared on the computer screen, and participants judged whether it was semantically related to the

preceding sentence (Cui & Herrmann, 2023; Kadem et al., 2020). Participants completed 5 blocks

(although 3 participants missed 1, 2, or 3 blocks of data due to incidental technical issues). Each block

comprised 36 trials (18 per SNR condition), and trials were pseudo-randomized such that a maximum of 2

trials of the same SNR could occur in direct succession. A 10-trial practice block preceded the experiment.

Behavioral performance in the semantic-relatedness task was calculated as the proportion of correct

responses. A paired-samples t-test was used to assess the difference between easy and difficult SNRs.

2.3 Recording of Stationary and Mobile Eye-Trackers

An Eyelink DUO was used as a high-precision stationary eye-tracker to record eye movements and

pupil size for both eyes at a sampling rate of 1000 Hz. We refer to this device as the "stationary" eye

tracker hereafter. A standard nine-point calibration and validation procedure (McIntire et al., 2014) was

performed at the beginning of each experimental block. A timestamp message was sent to the eye tracker

at the beginning of each babble onset. We used Pupil Labs Neon mobile eye-tracking glasses with a

Motorola Edge 40 Pro Android smartphone running the Neon Companion app (v2.8.2) (Baumann &

Dierkes, 2023) for data collection and management. We refer to this device as the "mobile" eye tracker

hereafter. Eye-movement and pupil-size data were recorded at 200 Hz, whereas head movement data were

collected at 110 Hz. The calibration for the mobile glasses involved two steps. First, each participant's

intraocular distance was measured and entered into the recording app. Second, participants completed a

brief, single-point calibration by fixating on a designated target. On the laptop that was used for stimulus

presentation, we also used SocialEyes software written in Python (Saxena et al., 2025) to remotely control

the smart phone and Neon Companion app (e.g., start and stop recording). We used SocialEyes' timestamp

synchronization procedure to estimate the offset between the internal clocks of the stimulus computer and

the recording smartphone (Saxena et al., 2025). Offsets between the two devices clocks were estimated

every 10-s during data collection for accurate timestamp calculation during offline analysis.

2.4 Eye-movement, pupil-size, and head-movement data processing

Data were processed offline using MATLAB and Python scripts. The x-coordinate, y-coordinate, and

pupil-size data from the stationary eye-tracking (EyeLink Duo) were down-sampled to 200 Hz to match

the sampling frequency of the eye data from the mobile eye-tracker. Mobile eye-tracking data (Pupil Labs

Neon) were corrected for lens distortion using built-in functions from the OpenCV library (Bradski, 2000).

Timestamps were estimated through linear interpolation using the recorded offsets between the

independent internal clocks of the stimulus computer and the recording smartphone (Saxena et al., 2025).

The remaining steps for data processing were similar for both eye trackers.

Pupil-size and x- and y- coordinate data were set to *NaN* (not a number in MATLAB) for 100-ms

before and 200-ms after each blink, as well as any outliers that deviated by more than 3 standard deviations

from the participant's block mean. All removed and missing data points (*NaN*-coded) were interpolated

using a shape-preserving piecewise cubic interpolation (*pchip*). Pupil-size data was then low-pass filtered at 5

Hz (FIR, 131 points, Kaiser Window).

We calculated gaze dispersion as a broad measure of eye movements. We recently developed this

measure to non-specifically capture any eye-movement changes associated with listening effort (Cui &

Herrmann, 2023; Herrmann et al., 2025; Herrmann & Ryan, 2024). Gaze dispersion was calculated as the

log-transformed standard deviation of gaze coordinates (averaged across x and y) within a 1-s sliding

window (ignoring data points that had been NaN-coded during preprocessing; and requiring at least 20

data points within a 1-s time window). A smaller value indicates fewer eye movements.

The continuous pupil-size and gaze-dispersion data were divided into epochs ranging from -1 s to 7

s time-locked to babble onset. Trials were averaged separately for easy and difficult SNRs. To enable

cross-device comparisons (stationary vs mobile), both pupil-size and gaze-dispersion time courses (using

across-trial average) were converted to within-participant z-scores, computed separately for the stationary

and mobile devices to account for scaling differences between devices. The pupil-size time courses were

then baseline-corrected by subtracting the mean in the pre-babble period [-1, 0] from all data points,

separately for each SNR condition (Mathôt et al., 2018; Winn et al., 2018b). Gaze-dispersion data do not

require baseline correction.

Gyroscope data from the mobile glasses were also analyzed to assess SNR effects on head

movements (gyroscope data are not available from stationary eye trackers). To this end, head-movement

data were analyzed similarly to gaze dispersion as positional variability, calculating the log-transformed

standard deviation of the gyroscope values (yaw, pitch, and roll) within a 1-s sliding time window. A lower

value indicates fewer head movements. Positional-variability data were divided into epochs ranging from -1

s to 7 s time-locked to babble onset, and averaged across trials for each SNR condition.

For statistical analyses, gaze dispersion and positional variability were averaged within the 1.5 s to 4

s (1.5 s corresponding to sentence onset; 4 s corresponding to the average sentence offset), separately for

the easy and difficult listening conditions. For the pupil size, data were averaged within the 2 s to 4.5 s to

account for the known delay in the pupil response (Knapen et al., 2016; Winn et al., 2018a, 2018b; Zhang

et al., 2022). Both pupil dilation and gaze dispersion were analyzed using a repeated-measures analysis of

variance (rmANOVA). This analysis included two factors: SNR (listening condition: easy vs. difficult) and

Eye Tracker (stationary vs. mobile). Pearson correlations were used to evaluate the consistency between

the two data from the two eye-tracking devices. A paired-sample t-test was used to assess SNR effect on

positional variability (head movements). Effect sizes for ANOVA are reported as omega squared (ω^2), and

for t-tests, as Cohen's d (d). All analyses were conducted using MATLAB and JASP software (version

0.95.1). Note that data from only 24 participants were available for the analysis of the pupil size. Pupil-size

data from two participants were not successfully uploaded to the Pupil Cloud, and could also not be

recovered offline.

3. Results

3.1 Behavioral Performance

As expected, behavioral performance accuracy was lower for the difficult (M = 0.77, SD = 0.08) than the

easy SNR condition (M = 0.93, SD = 0.05; $t(25) = 14.30$, $p = 2.78 \cdot 10^{-13}$, d = 2.8).

3.2 Pupil Size

The pupil size was larger in the difficult than in the easy condition (SNR effect: $F(1, 23) = 10.12$, $p = .004$,

$\omega^2 = .12$; Figure 2B). The main effect of Eye Tracker was not significant, $F(1, 23) = 3.66$, $p = .068$, nor was

the interaction, $F(1, 23) = 1.46$, $p = .238$, suggesting that the SNR effect on pupil size did not differ

between eye-tracking devices (see also Figure 2C). We confirmed that the SNR effect was indeed

significant for both devices (stationary: t(23) = 4.326, p = 2.78 · 10^{-13}, d = .88; mobile: t(23) = 2.285, p =

.032, d = .47). Pearson correlations indicated strong associations between the two eye trackers in both the

easy (r = .74, p < .001) and difficult (r = .88, p < .001) listening conditions, suggesting high consistency in

pupil size measurements across devices (see Figure 2D).

Fig. 2. Pupil responses to listening conditions for stationary and mobile eye trackers. (A) Time
courses of pupil size (in z-score (within participant); arbitrary units; a.u.) for stationary (left) and mobile
(right) eye trackers. Data are presented for difficult (−4 dB SNR; blue) and easy (+11 dB SNR; pink)
listening conditions, with the corresponding shaded areas representing standard error of the mean
(between-participant variance removed; (Masson et al., 2003)). Dashed lines denote babble onset (0 s), the
sentence onset (1.5 s) and average sentence offset (4 s). (B) Mean pupil size (averaged across 2–4.5 s) for
each condition and device. Asterisks denote statistical significance (p < .05). (C) Time course of the
difference in pupil size between SNR conditions for the stationary (orange) and mobile (green) eye
trackers. Horizontal lines at the bottom indicate time points of a statistically significant difference from
zero (i.e., significant SNR effect; p < .05; solid line = corrected using False Discovery Rate (Benjamini &
Hochberg, 1995); dashed line = uncorrected). (D) Scatter plots show the correlation between stationary
and mobile eye trackers for pupil size during difficult (left) and easy (right) conditions. Data points above
the diagonal line indicate that the mobile eye tracker measured a larger pupil size, while points below the
line show a larger pupil size measured by the stationary eye tracker.

3.3 Gaze Dispersion

Gaze dispersion was lower for the difficult compared to the easy listening condition (SNR effect: $F(1,25) =$

118.766, $p = 2.92 \cdot 10^{-11}$, $\omega^2 = .521$; Figure 3). The effect of Eye Tracker was not significant (F(1,25) = 0.28,

$p = .605$), nor the interaction (F(1,25) = 1.30, $p = .265$), suggesting gaze dispersion is similarly sensitive to

SNR for both device types. We confirmed that the gaze-dispersion effect was significant for the stationary

($t(25) = 9.889$, $p = 1.47 \cdot 10^{-10}$, d = 1.94) and the mobile eye tracker ($t(25) = 7.735$, $p = 1.01 \cdot 10^{-7}$, d = 1.52;

Figure 3C). Pearson correlations indicated moderate-to-strong correlations between the two eye trackers

for both the easy (r = .58, $p = .003$) and difficult SNR (r = .73, $p = 2.6 \cdot 10^{-6}$; Figure 3D).

Fig. 3. Gaze dispersion responses to listening conditions for stationary and mobile eye trackers.
(A) Time courses of gaze dispersion (in z‑score (within participant); arbitrary units; a.u.) for stationary
(left) and mobile (right) eye trackers. Data are presented for difficult (−4 dB SNR; blue) and easy (+11 dB
SNR; pink) listening conditions, with the corresponding shaded areas representing standard error of the
mean (between-participant variance removed; (Masson et al., 2003)). Dashed lines denote babble onset (0
s), the sentence onset (1.5 s) and average sentence offset (4 s). (B) Mean gaze dispersion (averaged across
1.5–4 s) for each condition and device. Asterisks denote statistical significance (p<.05). (C) Time course of
the difference in gaze dispersion between two conditions for the stationary (orange) and mobile (green) eye
trackers. Horizontal lines at the bottom indicate time points of a statistically significant difference from
zero (i.e., a significant SNR effect; p < .05 corrected using False Discovery Rate (Benjamini & Hochberg,
1995)). (D) Scatter plots show the correlation between stationary and mobile eye trackers for gaze
dispersion during difficult (left) and easy (right) conditions. Data points above the diagonal line indicate

that the mobile eye tracker measured a larger gaze dispersion, while points below the line show a larger
gaze dispersion measured by the stationary eye tracker.

3.4 Head Movements

Head movements – that is, positional variability – measured using the mobile eye-tracking glasses was

lower for the difficult compared to the easy SNR (t(25) = 2.97, p = .0064, d = .58; Figure 4).

Figure 4. Positional variability of head movements, measured by mobile eye-tracking glasses, index of listening effort. (A) Time courses of positional variability of head movements (in arbitrary units; a.u.). Data are presented for the difficult (-4 dB SNR; blue) and easy ($+11$ dB SNR; pink) listening conditions. Shaded regions represent the standard error of the mean (between-participant variance removed; (Masson et al., 2003)).

223 Vertical dashed lines mark the babble onset (0 s), sentence onset (1.5 s) and average sentence offset (4 s).
224 (B) Mean head movements (averaged across 1.5–4 s) for each condition. Lower values on the y-axis
225 indicate more stable head position. *p < .05.
226

3.5 Relationships Between Listening Effort Measures

Correlation analyses were conducted using the difference scores between the difficult and easy conditions

for each measure (i.e., SNR effect). There were no significant relationships between the listening effort

markers: SNR effects for gaze dispersion and pupil dilation were not correlated for Eyelink (r = -.20, p =

.34) nor Pupil Labs data (r = .04, p = .86). Further analyses using the data from the mobile eye-tracking

glasses (Pupil Labs) revealed a marginally significant correlation between positional variability (head

movement) and gaze dispersion (r = .39, p = .051) and a significant negative correlation with pupil dilation

(r = -.44, p = .026). Noteworthy, these correlation analyses were post-hoc, therefore, they might be

underpowered due to a small sample size (N=24).

4. Discussion

The current study investigated whether a pair of state-of-the-art mobile eye-tracking glasses are sensitive to

several physiological markers of listening effort. We found reduced gaze dispersion, increased pupil size,

and reduced head movements when speech masking – and thus listening effort – increased. Cross-device

comparisons found no significant differences in the speech-masking effect, although there was some

indication that the pupil-size effect may be numerically smaller for the mobile than the stationary eye-

tracker. Overall, the current results indicate high feasibility of using mobile eye-tracking glasses for the

assessment of listening effort, including head-movement measures that are not available using a stationary

eye-tracker.

4.1 Ocular and Head Markers

Both eye-trackers converged on the same pattern: as listening demands increased, gaze dispersion

decreased, whereas pupil size increased. These results are highly consistent with previous studies using

pupillometry (Almaraz et al., 2018; Piquado et al., 2010; Van Der Wel & Van Steenbergen, 2018; Zekveld

et al., 2018) and eye movements (Contadini-Wright et al., 2023; Cui & Herrmann, 2023; Herrmann et al.,

2025; Herrmann & Ryan, 2024) to assess listening effort. An increase in pupil size and a reduction in eye

movements appear to capture complementary but distinct aspects of listening effort (see also (Liu & Chait,

2025)): pupil size indexes effort through arousal involving the locus coeruleus-norepinephrine systems

(Joshi et al., 2016), whereas gaze dispersion may index effort through attentional control that suppresses

visual exploration, possibly relying on distinct neural systems, such as superior colliculus, thalamus, basal

ganglia, cerebellum, and the prefrontal cortex (Lencer et al., 2019; Pierce et al., 2019; Schneider et al., 2014;

Sparks, 2002).

Despite the use of a chin and forehead rest, participants still showed reduced head movements as the

listening task became more challenging. These results show that head movements persist despite the use of

a chin and forehead rest, and it still could be modulated by task demands. Furthermore, the reduction in

head movements during effortful listening suggests that individuals adopt a freezing or stabilization

strategy to free up cognitive resources. By reducing head movements, this strategy could minimize the

amount of proprioceptive information (Dault et al., 2001), thereby freeing up more cognitive resources for

processing acoustic information in the speech-in-noise task (Assländer & Peterka, 2014). This principle is

further supported by neurophysiological evidence from rodents, which shows that reduced body

movement is linked to heightened neuronal activity in the auditory cortex (Schneider et al., 2014). Critically,

although we observed a marginal correlation between head movements and eye-tracking measures (pupil-

size and gaze dispersion), it is unlikely that the SNR effect on gaze dispersion and pupil size are simple

artifact of head movements. For example, the mobile eye-tracking glasses are head-mounted, therefore, the

recorded eye movements was unaffected by head movements. Nevertheless, the relationship between head

movement and ocular changes presents an interesting area for future research.

4.2 Device Comparison

The effect of SNR (speech masking) on gaze dispersion was comparable across the stationary and the

mobile eye tracker. For pupil size, the SNR effect was numerically smaller for the mobile compared to the

stationary eye-tracker. However, neither the Device main effect nor the Device × SNR interaction was

significant, thus providing no formal evidence for a difference between devices. Without over-interpreting

the numerically smaller SNR effect for the mobile glasses, potential contributors could be the mobile

system's less precise calibration, less stringent luminance control (pupil size is highly light-dependent;

(Winn et al., 2018a) and head-worn geometry (Brisson et al., 2013; Hayes & Petrov, 2016), or generally a

lower sensitivity. Calibration for the mobile glasses was carried out once at the beginning of the

experiment, whereas the EyeLink eye tracker was calibrated prior to each block. Moreover, calibration

quality in head-worn systems could also degrade more rapidly over time, at least for older Pupil Labs

models and software (Ehinger et al., 2019).

Critically, in addition to finding no significant differences for the SNR effect between the EyeLink

and the Pupil Labs eye-trackers, individual participant data correlated between the two devices. This

suggests that state-of-the art mobile eye-tracking glasses, such as the Pupil Labs Neon, provide unique

opportunities to replace more expensive, stationary eye-trackers with mobile eye-tracking glasses without

much loss in sensitivity to assess listening effort. In fact, mobile eye-tracking glasses provide additional

benefits by measuring head movements, which also are indicative of listening effort.

4.3 Conclusion

The current study compared ocular markers of listening effort between a standard stationary and a modern

mobile eye-tracker. Both the stationary and the mobile eye-trackers showed increased pupil sizes and

reduced eye movements as listening became effortful, with no significant differences between the devices.

Mobile eye-tracking glasses additionally revealed reduced head movements under higher listening demand,

which is not available using stationary eye-tracking systems. The current study indicates that mobile eye-

tracking reliably captures listening effort, paving the path towards the assessments of listening effort in real

life.

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Author Declarations

Conflict of Interest:

The authors have no conflicts of interest to disclose.

Data Availability

The data that support the findings of this study are available from the corresponding author upon

reasonable request.

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