Transdiagnostic connectome-based predictive modeling of many behavioral phenotypes

reveals brain network mediators of clinical-cognitive relationships

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Abstract

Connectome-based predictive modeling (CPM) applied to functional MRI connectivity data can identify brain networks that vary with behavioral measures across subjects. The prediction strength also provides an index of how closely an external instrument relates to specific brain networks, potentially impacting their clinical interpretation. Here we use a deeply phenotyped transdiagnostic population ($n = 317$) to evaluate CPM performance across a variety of clinical and cognitive measures. The findings revealed a wide range of predictive performance for external instruments, with cognitive tests generally predicting better than self-reported clinical measures (unpaired t-test, $p < 0.001$). Testing the hypothesis that networks supporting cognition should be apparent in networks related to symptomatology, we examined the networks' overlap. The overlap was sparse, but primarily identified the thalamus, cerebellum, somatomotor networks, and the dorsolateral prefrontal cortex as key hubs in mediating relationships between clinical and cognitive measures. The findings reveal the extent to which external measures reflect underlying brain networks and highlight that examining network overlap can identify networks specific to clinically relevant cognitive dysfunction.

Introduction

Identifying neurobiological correlates of real-world behavioral measures can teach us about how certain neural dysfunctions manifest as clinical symptoms and cognitive deficits. Such information can improve precision psychiatry by increasing our understanding of the etiology of disorders, refining diagnostic and treatment strategies, and guiding novel therapeutic development. The recognition that many psychiatric symptoms and cognitive deficits exist on a transdiagnostic spectrum and stem from deviations from normal neural functioning led to the conceptualization of the NIMH's RDoC initiative[1,2]. In accordance with this framework, many studies have utilized functional MRI (fMRI) to link high-dimensional patterns of functional connectivity distributed across the brain to a wide range of continuous behavioral measures[3-9].

Connectome-based predictive modeling (CPM) is a well-established approach for linking behavioral measures to underlying brain networks measured by fMRI connectivity data[3,10] in a predictive modeling framework. The cross-validation employed in building the predictive models assures that the identified brain-behavior associations are generalizable[11]. A large body of work has demonstrated CPM's ability to relate functional networks to numerous cognitive and clinically relevant measures, such as sustained attention[5], memory[12], craving[13], PTSD[14], and social function[15]. A key assumption of the RDoC formalism is that a clinical symptom (like anxiety) should involve networks that vary with severity of the symptom and that the same networks generate the symptom independent of the patients' diagnostic category[2,16]. While numerous studies have shown that CPM can identify functional connectivity correlates for specific measures, few studies combine a large transdiagnostic sample with both extensive fMRI data and outside-the-magnet clinical and cognitive phenotyping. The data reported here provides an opportunity to assess the extent to which a wide range of diagnostically related clinical symptomatology measures (referred

to throughout as 'clinical measures') and cognitive instruments have clearly identifiable network

correlates and which do not in a clinically diverse transdiagnostic dataset[17]. Furthermore,

predicting an array of measures enabled us to address the extent to which measurement noise

influences prediction strength, which is an important consideration when interpreting brain-based

predictive models[18].

The human brain consists of many complex networks that support a diverse array of traits. CPM

can be used to map the functional network architecture underlying a variety of clinical and

cognitive measures thus providing a means to assess network commonalities. The RDoC

framework suggests that disordered circuits can affect both diagnostically-related symptoms and

cognitive abilities. This is corroborated by a large body of evidence indicating that cognitive

deficits often co-occur with psychiatric symptoms[19]. However, disordered circuits vary

substantially across individuals[20], and may not completely impinge on a network related to a

particular symptom or cognitive process. Rather, an individual's disordered circuits are more likely

to partially affect multiple networks linked to various symptom and cognitive measures. This

phenomenon may underlie the highly variable cognitive deficits seen in psychiatric

populations[16,19]. According to this hypothesis, individuals with disordered circuits impinging on

networks related to both symptoms and cognition should experience cognitive deficits that co-

occur with symptomatology, while individuals with disordered circuits impinging on networks only

related to either symptoms should have psychiatric symptoms without cognitive deficits (or vice

versa). While it is unlikely that any disordered circuits would overlap completely with a specific

symptom or cognitive network, brain-behavior modeling provides a means for assessing the

effects of a partial overlap. Therefore, we sought to identify where the networks impacted by

clinically relevant symptomatology overlapped with networks supporting cognition. Given that

patients who experience cognitive impairment may respond differently to various forms of

treatment than unimpaired patients[21-23] and that psychiatric patients often consider cognitive

impairments among their primary priorities for treatment[24,25], identifying the loci of these

interactions is an important research focus that could lead to novel diagnostic biomarkers and

precision treatment targets. Furthermore, this would provide a putative link between

inconsistencies in cognitive perturbations[16,19] and high inter-individual variability in network

dysfunctions seen in psychiatric populations[20].

This study has two primary goals. First, we determine which of the many clinical and cognitive

measures obtained using a comprehensive testing battery administered outside the magnet yield

CPM models with high prediction strength and which do not. This allows us to characterize the

degree that each measure reflects the functioning of identifiable brain networks and to compare

prediction strength across measures (i.e., the correlation between observed and predicted

values). Second, we utilize the networks revealed by CPM in the first aim to examine where the

networks implicated in clinical symptomatology overlap with networks that support cognitive

functioning. By doing so, we demonstrate how CPM can precisely locate functional networks that

mediate relationships between symptoms and cognition. This approach improves the specificity

of mapping networks to behavior by highlighting subsets of edges within networks associated with

clinical symptomatology that co-fluctuate with cognitive dysfunction.

Results

In the present study, we utilized a demographically and clinically diverse transdiagnostic

population[26] (n=317; demographic data is presented in **Supplemental Table 1**). The dataset

consists of fMRI data from 2 resting-state and 6 task runs, as well as questionnaires collected

outside the magnet consisting of 7 real-world self-report clinical assessment scales comprised of

a total of 63 distinct measures, and 6 neuropsychological tests yielding 28 distinct cognitive

performance measures. The clinical assessment instruments were the Adult Temperament Questionnaire (ATQ)[27], the Behavior Rating Inventory of Executive Function (BRIEF)[28], the Brief Symptom Inventory (BSI)[29], the Interpersonal Reactivity Index (IRI)[30], the Positive and Negative Affect Schedule (PANAS)[31], the Pittsburgh Sleep Quality Index (PSQI)[32], and the Perceived Stress Scale (PSS)[33]. The cognitive testing instruments were the verbal fluency, trail making, color-word interference, and twenty questions subtests from the Delis-Kapan Executive Function Scale (D-KEFS)[34], the letter-number sequencing, symbol search, and cancellation subtests from the Wechsler Adult Intelligence Scales (WAIS)[35], the vocabulary and matrix reasoning subtests of the Wechsler Abbreviated Scale of Intelligence 2nd Edition (WASI)[36], the finger windows and list learning subtests of the Wide Range Assessment of Memory and Learning 2nd Edition (WRAML)[37], the reading subtest of the Wide Range Achievement Test 5th Edition (WRAT)[38], and the Boston Naming Test 2nd edition (BNT)[39]. The fMRI data was preprocessed with standard preprocessing methods (described in greater detail in **Methods** and Ref 26). The Shen 268-node atlas[40] was applied to the preprocessed data, parcellating it into 268 functionally coherent nodes, and functional connectivity matrices were derived for each participant/run. The averages of all 8 functional connectivity matrices were computed for each participant and used as input in building the CPMs. CPM was run for all clinical and cognitive measures in a 10-fold cross validation. Prediction strength was quantified as the Spearman correlation (ρ) between the observed measurements and the predicted values. Significance was determined by comparing the prediction strengths from 1000 CPM permutations to a null distribution generated from running CPM on randomly permuted observations. The proportion of null predictions that exceeded the median prediction strength represented the predictive models' *p*-values. All *p*-values were FDR corrected for multiple comparisons.

Prediction strength of clinical measures

To determine whether a measure had sufficient prediction strength to yield reliable brain network

correlates, measures must have had *pFDR* < 0.05 and prediction strength > 0.1. In neuroimaging,

prediction strengths of 0.1 are generally considered weak, but are accurate enough if also

statistically significant to yield meaningful insights about the neurobiological features important to

these models[41]. Of 63 clinical measures, 38 (60.32%) met our criteria for being predicted strongly

enough to have identifiable whole brain functional connectivity networks (**Fig 1**). The other 25

measures failed to yield sufficient prediction strength to continue with further analyses. When

examining predictive model performance across scales and measures, several notable patterns

emerged. Of the 7 clinical assessment scales, models built with measures related to sleep quality

tended to have the highest prediction strength, with 5 of the top 10 strongest predictions belonging

to the PSQI. The mean prediction strength across all PSQI measures was $\rho = 0.170$. Measures

pertaining to positive affect from the PANAS also yielded strong predictive models, with 5 out of

6 of these measures providing reliable network correlates (mean $\rho = 0.151$). PANAS measures

related to negative affect tended to yield slightly lower prediction strength, with 4 out of 7 providing

reliable network correlates (mean $\rho = 0.120$). $\rho\rho\rho\rho\rho\rho$Prediction strength values and associated

prediction *p*-values can be found in **Supplemental Table 2**, and distributions of clinical measures

can be found in **Supplemental Fig 1**.

Interestingly, there were 4 separate instances where the same measures quantified by different

assessment scales yielded widely different predictions. The prediction strength for 'fear' was

significantly higher when measured by the ATQ than when measured by the PANAS ($\rho = 0.239$

vs $\rho = 0.105$; paired t-test: $t(999) = 192.12$, $p < 0.001$), as was 'sadness' ($\rho = 0.165$ vs $\rho = 0.099$;

paired t-test: $t(999) = 88.63$, $p < 0.001$). PANAS 'hostility' was better predicted than BSI 'hostility'

($\rho = 0.181$ vs $\rho = 0.123$; paired t-test: $t(999) = 98.23$, $p < 0.001$). Furthermore, the prediction

strength for 'positive affect' was higher when measured as an index of all measures related to

positive affect by the PANAS than when assessed as a single measure by the ATQ ($\rho = 0.164$ vs

$\rho = 0.122$; paired t-test: $t(999) = 54.26$, $p < 0.001$).

Prediction strength of cognitive measures

Nearly all cognitive measures yielded strong prediction strength by CPM. Successful models were

built for 26 of 28 (92.86%) measures from the cognitive panel (**Fig 2**). The matrix reasoning test

from the WASI provided the model with the highest prediction strength ($\rho = 0.428$). Predictions of

measures from the D-KEFS were highly variable, though all produced (range: $\rho = 0.159$ to $\rho =$

0.374). In general, measures from the twenty-questions (mean $\rho = 0.288$) and trail-making tests

(mean $\rho = 0.320$) were the most strongly predicted measures from D-KEFS. Performance

measures from the WAIS (mean $\rho = 0.319$), the WRAML (mean $\rho = 0.263$), and the WRAT ($\rho =$

0.302) were generally predicted strongly. Measures from the BNT (mean $\rho = 0.224$) and the D-

KEFS verbal fluency test (mean $\rho = 0.177$) were predicted less strongly. The two cognitive

measures that CPM did not generate reliable models for (WRAML verbal learning intrusion and

BNT number correct following a stimulus cue) had the highest percentage of individuals

performing at ceiling (see **Supplemental Fig 2**; 53.16% and 77.19%, respectively). These results

highlight that predictive models linking external trait measures to brain connectivity patterns via

CPM can be built across a wide range of cognitive metrics, with higher prediction strengths

representing greater confidence in the derived network correlates. Prediction strength values,

associated prediction p-values, and brief descriptions of the cognitive abilities theoretically tested

by each measure can be found in **Supplemental Table 3**.

What drives prediction strength?

In addition to CPM significantly predicting a higher percentage of cognitive than clinical measures,

the prediction strength of the cognitive measures that were successfully modeled were higher

than the clinical measures' (**Supplemental Fig 3**; cognitive measures' mean prediction strength:

ρ = 0.289; clinical measures' mean prediction strength: ρ = 0.168; $t(62)$ = 8.39, $p < 0.001$). This

highlights that CPM yields more accurate and robust functional network correlates for cognitive

than for clinical measures.

We next sought to understand the factors that influence model performance leading to better

prediction strength for some measures compared to others, noting that the functional connectivity

data remained constant across all models. Due to the differences in prediction strength between

clinical and cognitive assessments, we examined how prediction strength varied across

instruments and subdomains tested in clinical and cognitive assessments separately. One-way

ANOVAs revealed that prediction strength strongly varied as a function of instrument/subdomain

for clinical (**Fig 3a**; $F(13,62986)$ = 3059.98, *Cohen's F* = 0.795, $p < 0.001$) and cognitive measures

(**Fig 3b**; $F(13,27986)$ = 1194.96, *Cohen's F* = 0.745, $p < 0.001$).

Recent work questioned the extent to which brain-based predictive modeling is influenced by

measurement noise[18]. To address this, we tested whether the predictive accuracy on these

measures was related to their intraclass coefficients (ICCs) reported by the manuals and seminal

papers describing each of the testing instruments. We also examined whether model performance

was related to other characteristics of the measures' data (distribution skewness and variance).

Clinical prediction strength was not correlated with ICC in the measures with reported ICC values

(r = 0.026, *pFDR* = 0.802), nor was it related to the measures' skewness (r = 0.072, *pFDR* =

0.802) or variance (r = 0.032, *pFDR* = 0.802) (**Fig 3c**). Similarly, cognitive prediction strength was

not correlated with ICC in the measures with reported ICC values (r = -0.122, *pFDR* = 0.802), nor

was it correlated with skewness (r = -0.456, $pFDR$ = 0.108) or variance (r = 0.262, $pFDR$ = 0.534)

(**Fig 3d**). Together, these results suggest that CPM performance depends on how well the scale

captures aspects of cognition or clinical symptoms and how tightly coupled these measures are

to brain organization. The differential results across tests do not appear to be significantly driven

by measurement stability or distribution of scores across subjects.

Network similarity across measures

Since disordered circuits could impinge upon both clinical and cognitive networks, we examined

the degree of overlap between predictive networks for all clinical and cognitive measures (**Fig 4**).

This was achieved by sorting the predictive networks based on similarity using an agglomerative

hierarchical clustering algorithm. As expected, the similarities between the measures' networks

mirrored the correlational structure of the measures themselves since the networks are derived

from the measures. In general, the clinical measures were most related to other clinical measures,

while the cognitive measures were most related to other cognitive measures. The only exception

was high intensity pleasure (ATQ), which was more closely related to cognition than to other

clinical measures. The Dice similarity between clinical-cognitive networks was generally much

lower than between clinical-clinical (unpaired t-test: t(788.66) = -31.68, $p < 0.001$) and cognitive-

cognitive networks (unpaired t-test: t(389.11) = -23.39, $p < 0.001$). Additionally, after adjusting for

multiple comparisons using an FDR correction, only 101 pairs of clinical-cognitive measures were

significantly correlated ($pFDR < 0.05$). Together, this suggests that brain networks that vary as a

function of cognitive performance are largely distinct from those networks that vary systematically

with clinically relevant symptomatology.

We then grouped the brain networks predicting clinical and cognitive measures into 9 clusters

based on the hierarchical clustering results. This number was determined using the elbow

method[42] (**Supplemental Fig 4**), which is a commonly used approach for determining an

appropriate number of clusters to group data into. These clusters were selected to visualize how

the measures grouped together based on network similarity, and to compare the regions

important in driving CPM predictions across clusters, rather than to make a claim about how many

clusters exist in this dataset. The patterns that the CPM networks loaded onto each of the 9

clusters corresponded to what the measures theoretically assess. Of these 9 clusters, 5 were

composed of clinical measures and 4 were composed of cognitive measures. For discussion

purposes, each of the clusters were given a name that generally reflects the broad measures

composing them. The cluster labels are displayed underneath the dendrogram in **Fig 4**, which

align with the sorted measures displayed in the matrix below. It is important to note that these

names do not encompass all the behavioral phenotypes present in each cluster. Additionally,

since they were not orthogonal, important features were often shared across clusters. For

example, cognitive control abilities were likely important to performing all cognitive tests, not just

the tests in the 'cognitive control' cluster. This phenomenon is reflected by the substantial overlap

in the network features between clusters.

Localizations of networks important to predictions

We examined the contributions of specific networks to prediction strength of clinical measures

using the canonical Yeo17 networks as a reference[43] (**Fig 5a**). For identifying the nodes and

edges important to predictions across clusters, we compared positively predicting network

features from the positive affect cluster to negatively predicting network features from the 4 other

clinical clusters (and vice versa) because these cluster's measures were anticorrelated. Doing so

allowed us to effectively put the brain correlates of measures where higher scores indicated better

mental health on the same scale as measures where higher scores indicated worse mental health.

The nodes driving the prediction strength for the clinical measures displayed substantial overlap

across the clinical measures' clusters for both positively (mean pairwise Jaccard similarity = 0.252

+/- 0.088 SD, one-tailed $p < 0.001$) and negatively predicting nodes (mean pairwise Jaccard

similarity = 0.188 +/- 0.068 SD, one-tailed $p < 0.001$). Examining the top 10% highest degree

nodes in each cluster's predictive networks revealed that the thalamus was the only region

important to positively predicting every cluster of clinical measures, and only the cerebellum

contained nodes that were important to negatively predicting each cluster of clinical measures. A

full list of the top 10% highest degree positive and negative predicting nodes for each clinical

measure cluster can be found in **Supplemental Tables 4 and 5**. Many of the same nodes that

were important in positive predictions were also implicated in negative predictions (Jaccard

similarity = 0.500, one-tailed $p < 0.001$). Furthermore, examining the top 10% of canonical network

pairs where the predictive edges were most concentrated showed that limbic A to brainstem

connectivity was important to all positive predictions, while within somatomotor A/B and

somatomotor A to dorsal attention B were important to negative predictions across all clinical

measures' clusters.

Similarly, the networks supporting prediction strength in the cognitive measures were assessed

(**Fig 5b**). As with the clinical measures, we flipped the sign of the cognitive measures' predictive

networks before comparing across measures to ensure that all positively predicting networks were

indicative of better performance on the task, and not just a higher score, since sometimes a higher

score was undesirable. The nodes contributing to predicting cognitive measures displayed

substantial overlap across the cognitive measures' clusters for both positively (mean pairwise

Jaccard similarity = 0.197 +/- 0.092 SD, one-tailed $p < 0.001$) and negatively predicting nodes

(mean pairwise Jaccard similarity = 0.210 +/- 0.118 SD, one-tailed $p < 0.001$). Despite this,

examining the top 10% highest degree nodes in each cluster's predictive networks showed that

only nodes within the visual A and somatomotor B networks were positively associated with

cognitive performance and only one node in the temporal parietal network was negatively

associated with cognitive performance across all clusters. A full list of the top 10% highest degree

positive and negative predicting nodes for each cognitive measure cluster can be found in

Supplemental Tables 6 and 7. There was significant overlap between the nodes important to

positively and negatively predicting cognitive measures (Jaccard similarity = 0.294, one-tailed *p*

< 0.001), and these nodes often were in the cerebellum. However, this overlap was less

pronounced than it was in the clinical measures (Jaccard similarity = 0.294 vs 0.500). The nodes

that were only important to positive predictions were typically located toward the bottom of the

functional gradient in lower-level unimodal cortex, while nodes that were only important in

negative predictions were frequently localized near the top of the functional gradient in higher-

level transmodal cortical regions[44] (see **Supplemental Fig 5**). Examining the top 10% of canonical

network pairs where the predictive edges were most concentrated showed that dorsal attention A

to dorsal attention B, default mode A to cerebellum, limbic A to limbic B, somatomotor A/B to

cerebellum, and visual A to somatomotor B network connectivity was important to positive

predictions across all cognitive measures' clusters. Furthermore, dorsal attention B to default

mode A, default mode B to temporal parietal, somatomotor A/B to dorsal attention B, somatomotor

B to default mode A, and within somatomotor A network connectivity were important for driving

negative predictions across all cognitive measures' clusters.

Networks mediating clinical-cognitive relationships

In **Fig 4** we highlighted that the correlations were relatively weak, and network overlaps were

sparse between clinical and cognitive measures. However, given that cognitive alterations co-

occuring with psychiatric symptomatology are hypothesized to emerge from disordered circuits

that span both systems, we sought to determine where these network overlaps are located, and

if their connectivity mediates relationships between significantly correlated pairs of clinical and

cognitive measures (pFDR < 0.05). This was achieved using the sum the overlapping edges'

connectivity as the mediator variable in mediation analyses for each of the 101 significantly

correlated clinical-cognitive measure pairs (**Fig 6a**). We did not have an *a priori* hypotheses

regarding the directionality of these mediations, so we conducted two mediation analyses for each

pair of correlated clinical-cognitive measures. In one, the clinical measures were the dependent

variables, and the cognitive measures were the independent variables, and in the other, the

dependent and independent variables were switched. The mediation analyses were significant (*p*

< 0.01) bidirectionally for all 101 pairs of clinical-cognitive relationships examined (**Fig 6b**). For

each clinical-cognitive relationship pair, we reported the larger of the two indirect mediation

coefficients.

We then examined the localization of these mediating networks by grouping them by the clusters

that each pair of related measures belonged to (**Fig 6c**). Even within the same pairs of clusters,

the edges in the shared clinical-cognitive networks showed little overlap. However, the nodes

implicated in the shared networks were highly consistent across clinical-cognitive measure pairs.

The nodes and important canonical network-network connections involved in generally mediating

clinical-cognitive relationships are highlighted in **Fig 7**. Of the top 10% highest degree nodes

important to mediating clinical-cognitive relationships, 8 were in the cerebellum, 6 were in the

somatomotor networks, 2 covered the thalamus (bilaterally), 2 were in frontoparietal control C

(bilateral dLPFC), 2 were in brainstem, and 1 was in each the ventral attention B, dorsal attention

B, limbic A, and default mode B. A full list of these nodes and the MNI coordinates of their

centroids can be found in **Supplemental Table 8**. Interestingly, the first and third highest degree

nodes were the left and right thalamus (respectively), while 6 out of the 10 highest degree nodes

were in the cerebellum. Examining the top 10% canonical network pairs where the mediating

edges were concentrated corroborated these results. Most of these mediating edges were

concentrated between the cerebellum and subcortical nodes (e.g., the thalamus), between

cerebellum and somatomotor networks, within somatomotor networks, between somatomotor and

subcortical regions (thalamus), and between somatomotor and higher order networks (e.g.,

frontoparietal control C (dLPFC), default mode B, dorsal attention B, ventral attention B, limbic A).

These results highlight the importance of the cerebellum, the thalamus, somatomotor cortices,

and bilateral dLPFC in generally mediating clinical-cognitive relationships.

Discussion

This study had two primary goals. First, we aimed to comprehensively evaluate which clinical and

cognitive measures reflect clear brain correlates as determined by prediction strength in CPM.

The findings showed that, in general, there is a tighter coupling between brain networks and

external instruments for cognitive tests compared to clinical measures. We also show that this

relationship is not uniform across measures, as prediction strength varied substantially across

measures in both classes and was not driven by differences in measurement stability. Our second

goal was to test a hypothesis upon which the RDoC framework is based: that evidence for

disordered circuits should be apparent in both cognitive and clinical measures. Our results

indicated that the networks implicated in clinical symptomatology impinge upon networks that

support cognitive functioning, and that specific networks mediate relationships between clinically

relevant symptoms and cognitive performance metrics. As might be expected, the networks

associated with symptoms do not cleanly overlap with any specific cognitive network. This work

further establishes a framework for how to use brain-behavior modeling to locate functional

networks that support and facilitate relationships between multiple behavioral domains.

Clinical predictions and associated networks

The broad testing of clinical measures that we employed in this study allowed us to systematically evaluate the extent to which a variety of clinical assessment instruments reflect brain network functioning. We identified reliable functional connectivity correlates of many clinical measures collected in this dataset (38 out of 63 predicted at $\rho > 0.1$ and $pFDR < 0.05$). Varying prediction strength between instruments highlights that some clinical assessment tools are better suited to capture brain network functioning than others. Among these, the PSQI, the BRIEF (behavioral regulation measures), PANAS, ATQ (non-aggressive negative affect measures) and BSI all tended to be well modeled in the brain. Conversely, measures from the IRI, BRIEF (metacognition measures), ATQ, and the PSS did not consistently yield reliable brain network models.

Each of these clinical assessment instruments utilized self-reporting. The subjective nature of self-reports introduces several confounds that could interfere with CPM prediction strength, such as response style differences related to introspection abilities[45], social[46] and cultural backgrounds[47], or differences in how respondents and assessment administrators interpret the questions[48]. Measures that are less prone to these influences are thus more likely to have clear network correlates. Understanding how to refine self-report scales to yield better behavioral predictions will improve the extent to which they reflect network functioning, thereby enhancing their utility in identifying neural generators of clinical dysfunction.

The considerable overlap in the networks important to predicting all clinical measures suggests that CPM was capturing a low-dimensional general factor of psychopathology (p-factor) posited by the HiTOP framework and elsewhere[49,50]. Each cluster's unique deviations from this general

p-factor network, therefore, track network dysfunctions specific to the clusters' phenotypic

makeups. Our results strongly implicate the thalamus and cerebellum as key nodes in this p-factor

network. These brain structures and their clinical relevance are commonly overlooked, and

researchers have argued that this omission is stifling progress in neuroscience[51]. However, there

is evidence suggesting the functional connections involving the cerebellum and thalamus contain

clinically relevant information[52,53]. Although not involved in predicting clinical measures across all

clusters, nodes within the somatomotor network were also frequently involved in predicting clinical

measures. Like the cerebellum and deeper brain structures such as the thalamus, the

somatomotor network has also been relatively overlooked in psychiatric research. An emerging

body of research has linked somatomotor network dysfunction to clinical pathology[54-57]. Our

results add to this mounting evidence implicating the thalamus, cerebellum, and SM network in

symptomatology.

Cognitive predictions and associated networks

We also evaluated a comprehensive battery of cognitive tests to identify the extent to which they

reliably reflect brain network functioning. Nearly all cognitive measures yielded models with good

prediction strength (26 out of 28 predicted at $\rho > 0.1$ and $pFDR < 0.05$). More than 50% of

participants performed at ceiling for the two measures that were not modeled well (verbal learning

intrusion (WRAML) and number correct following a stimulus cue (BNT)). These were also the two

cognitive measures with the lowest range of scores (see **Supplemental Fig 2**). These results

highlight the importance of utilizing cognitive tests with a sufficiently wide distribution of scores to

identify reliable functional network associations of cognition. However, considering that there was

not a significant correlation between measurement score variance and prediction strength across

all cognitive measures (see **Fig 3**), the distribution of the scores likely only affects prediction

performance up to a certain extent.

Since the cognitive tests utilized objective response time- and accuracy-based performance

metrics, they were not susceptible to the biases mentioned previously to the same degree as

subjective self-report measures. This was likely a major factor contributing to their prediction

strength being substantially higher than the clinical measures' (clinical measures' mean $\rho = 0.168$;

cognitive measures' mean $\rho = 0.289$). It is also possible that the networks that support cognition

are less variable than the ones that support psychiatric symptoms, or that the instruments used

to model symptoms are more flawed and reflect brain functioning to a lesser extent than cognitive

tests. Both possibilities could contribute to this difference in prediction strength. Regardless, the

higher prediction strength for cognitive tests is accompanied by greater confidence in derived

brain network correlates.

The networks that predicted cognitive measures also showed considerable overlap with each

other, suggesting that these common networks track with the g-factor commonly reported in the

literature[58]. Given that all the tests probe numerous cognitive processes, this g-factor network

likely reflects a mix of the various cognitive components that interact with each other to facilitate

test performance. The nodes important for positively predicting cognitive performance often lied

at the opposite end of the principal cortical functional gradient[44] from negatively predicting nodes,

highlighting a departure from the nature of clinical networks, where the same nodes were often

important to positively and negatively predicting measures. Interestingly, this pattern did not apply

to cerebellar nodes, as areas of the cerebellum that were involved in positively predicting

cognition were also commonly involved in negatively predicting cognition. Furthermore, our

findings also strongly implicate the SM network in supporting cognitive functioning, in line with the

recent report that systems supporting higher-order cognition are interdigitated within motor

cortex[59].

Other factors contributing to prediction strength

Recent work has suggested that measurement stability, as reflected by ICC, is a major component

underlying predictive modeling performance[18]. We directly tested this by correlating the prediction

strength of clinical and cognitive measures with the ICCs reported by the authors of those scales.

We observed a very strong effect of instrument/subdomain on predictions, while an effect of ICC

was absent across all measures, including those that failed to model well (see **Fig 3**). This does

not rule out the possibility that measurement stability is an important factor contributing to brain-

based predictive modeling success. Rather, it suggests that if a measurement is sufficiently

stable, then we can generate a valid brain-behavior model. Most of the ICC values in the

measures we used were high (>0.6). Thus, the effect that this could have had on prediction

performance would be minimal, and the effect of the phenotype dominates.

Additionally, CPM can directly test how the development of the measures can lead to measurable

differences in the extent to which they engage clear brain correlates[60]. As demonstrated here,

there were 4 instances where different instruments provided measurements with the same label

that purportedly measured the same phenotype but yielded widely different predictions (see **Fig

1**). These findings highlight how the framing of the questions probing symptoms or how index

scores composed of multiple related measures can improve the confidence of the network

correlates derived from predictive modeling.

Relationships between clinical and cognitive measures

While a large body of work has demonstrated cognitive deficits in psychiatric populations, the findings here indicate that the relationships between symptom and cognitive measures were weak (maximum $\rho = 0.234$, minimum $\rho = -0.227$). Only 10.22% of clinical-cognitive measure pairs were significant after correcting for multiple comparisons. Furthermore, the effect sizes of the relationships that were significant were small. Given that the ICC values for these measures were all greater than 0.6, this finding is probably not a result of measurement noise, but rather likely reflects the highly variable cognitive alterations within clinical populations[16,19,21,22].

When examining the clinical-cognitive relationships more closely, some interesting patterns arose. Significant correlations between clinical and cognitive measures were evenly distributed across clusters, suggesting that these measures might be related through more general p- and g-factor correlations. However, not all clinical measures were associated with poorer cognitive performance. In fact, better performance on cognitive tests that contained a language component (e.g., the BNT) were typically correlated with worse affect. This positive association with the BNT extended to depression symptoms. One potential interpretation of this finding could be that enhanced verbal abilities feed into more ruminative thoughts and higher levels of depression symptoms[61]. Interestingly, depression symptoms were also negatively associated with performance on WAIS digit symbol coding, a test that assesses cognitive control. This dissociation between how depression symptoms were positively correlated with lexical retrieval (as assessed by BNT) but negatively correlated with cognitive control could provide useful information for studies investigating ways to identify depression biotypes. The implications of how this can inform precision medicine frameworks should be further explored, especially in light of recent evidence that cognitively impaired depression patients respond differently to antidepressants than patients without cognitive impairment[21].

Shared networks mediate clinical-cognitive relationships

Mirroring the correlations between clinical and cognitive measures, the network overlaps were also sparse. This finding is consistent with a recent report that predictive network features are distinct across mental health and cognitive measures[62]. Our results extend these findings by revealing that these sparsely overlapping networks mediate clinical-cognitive relationships. These findings suggest that varying degrees of dysfunction within overlapping networks could explain the heterogeneous cognitive deficits seen in psychiatric populations[16,19,21,22]. This aligns with the RDoC hypothesis stating that disordered circuits within an individual likely do not impinge directly on a single network, but instead, they partially affect multiple networks linked to various symptoms and cognitive measures. Identifying these overlapping networks can guide cognitive intervention personalization in clinical populations, which often assume that symptomatology stems from cognitive deficits[19] and that cognitive remediation can improve symptoms[63].

Even though significant clinical-cognitive relationships were mostly evenly spread across cluster-cluster pairs, nodes localized to the thalamus, cerebellum, and somatomotor network were most important in mediating these relationships. Bilateral dLPFC was also involved, corroborating recent findings that individuals with treatment resistant depression who also have cognitive impairments respond better to TMS applied to dLPFC than patients with intact cognition[22]. Additionally, evidence has emerged recently suggesting that the thalamus, cerebellum, and somatomotor networks may be promising treatment targets for a variety of symptoms across several populations, such as depression, psychosis, and obsessive-compulsive disorder[64-69]. Interestingly, although the thalamus and cerebellum were not necessarily the most important nodes to predicting cognitive performance measures, our results suggest they were the most important hubs for generally maintaining clinically-relevant cognitive functioning. Future work

should further examine whether neuromodulation or selective pharmacological manipulation

targeting neurons in these areas can effectively improve cognitive deficits in psychiatric

populations. The patterns by which individual pairs of overlapping clinical-cognitive networks

deviated from this common mediating network may provide additional translational insights, such

as which networks underlie the opposing relationships between depression symptoms and lexical

retrieval versus cognitive control.

This study highlights how this approach can be useful for refining networks identified by brain-

behavior modeling to pinpoint the specific networks that track with cognitive deficits co-occurring

with clinical symptomatology. Our findings corroborate a growing body of literature highlighting

that the thalamus, cerebellum, somatomotor network, and dLPFC are important to both clinical

symptomatology and cognition. Studies probing the causal nature of these relationships and their

implications in precision medicine are warranted.

Limitations

There are some noteworthy limitations to the current study. First, without an external sample to

validate our results, we cannot be certain that the network correlates of various behavioral

measures will generalize to unseen data. This is one of the first studies to have a large

transdiagnostic sample, extensive fMRI data (>48 min), and comprehensive phenotyping

conducted outside the magnet. Therefore, similar data to evaluate whether these results

generalize is lacking. Second, some of the studies that we obtained ICC values from were

inconsistent in the time intervals between test and re-test, sample sizes, and age groups utilized.

These differences could have biased ICC values, potentially obscuring any effects on prediction

accuracy. Third, we acknowledge that there are many different methods to determine "optimal"

clustering solutions that each typically yield widely different results, and that there is often no clear

determination of how many clusters exist[70]. The clustering performed here was solely intended

for reducing the dimensionality of the data and showing how similar the measures were to each

other based on their network correlates. Their labels were therefore only used to help describe

the types of measures composing each cluster. Fourth, the biases introduced via self-reporting

reduce the prediction strength of clinical measures and add noise to our network estimates for

those measures. However, most instruments available for assessing psychiatric symptoms in

clinical contexts rely on self-reporting, and objective assessments are lacking. Finally, our results

beg a deeper investigation into the relationship between symptoms and cognition. We have

assumed here that these measures reflect fixed traits, but it is well known that symptoms and

cognition wax and wane in clinical populations. Understanding how these models may vary, and

how the relationship between symptoms and cognitive variables interact over time could be very

informative in clinical contexts[71].

Methods

Participants

The sample reported in this study includes data from 317 demographically diverse participants

with at least 48 minutes of high-quality functional MRI data and extensive phenotyping outside of

the magnet. Participants were recruited from advertisements broadly distributed throughout the

New Haven community and referrals from Yale clinics. This transdiagnostic population

experienced a wide range of symptoms and symptom severities, often with multiple psychiatric

diagnoses. All participants provided written informed consent in accordance with a protocol

approved by the Yale IRB. A more thorough description of this dataset can be found elsewhere[26].

Imaging acquisition protocol

The imaging data was collected at Yale on a 3T Siemens Prisma scanner with a 64-channel head

coil. A high-resolution T1-weighted MPRAGE (TR=2,400 ms, TE=1.22 ms, flip angle=8°, voxel

size 1 mm^3) was acquired for each participant. The functional data were obtained using a

multiband EPI sequence (TR=1,000 ms, TE=30 ms, flip angle=55°, slice thickness=2 mm,

multiband factor=5). A total of 6-task and 2-resting-state runs were acquired, each lasting 6

minutes and 49 seconds. The first and last functional scans were resting-state runs. The six task

runs were all designed as event-related designs and comprised a working memory (n-back), an

inhibition (stop signal task), a decision making (card guessing), an emotional perception (eyes),

a continuous performance task (the gradCPT), and a more naturalistic movie watching task. The

task order was randomized and counterbalanced across participants. There was no block

structure to the tasks and they were designed as state-manipulation tasks for functional

connectivity analyses unlike a typical task paradigm designed for conventional GLM analyses.

We ensured that participants understood task instructions and received practice. Responses were

recorded on a button box. Analyses were restricted to participants who completed all fMRI scans

runs.

Functional MRI data processing

Skull stripping of the structural scans was done using an optimized version of the FMRIB's

Software Library (FSL) pipeline[72,73]. Motion correction was done using SPM12[74]. Nonlinear

registration of the MPRAGE to the MNI template was performed using BioImage Suite[75], and

linear registration of the functional to the structural images was done through a combination of

FSL[76] and BioImage Suite. The remaining preprocessing steps were performed in BioImage

Suite, including global signal regression, high-pass and low-pass filtering, and regression of

motion parameters. All registered data were visually examined to ensure whole-brain coverage,

adequate registration, and the absence of artifacts or other quality issues. Subjects were included

in the study if they completed all eight fMRI scan runs and had a grand mean frame-to-frame

displacement of less than 0.15 mm and a maximum mean frame-to-frame displacement of less

than 0.2 mm. Two participants were scanned with a slightly shorter scanning time (25 seconds

shorter) and were included in the dataset.

The Shen 268 node atlas[40] was applied to the preprocessed data, parcellating it into 268

functionally coherent nodes. Pearson correlations of the time series between all node pairs were

computed and subsequently z-transformed to generate 8 functional connectivity matrices for each

participant. The averages of all functional connectivity matrices were computed for each

run/participant. Since individuals' functional connectomes are more similar to themselves,

regardless of the task, than they are to other individuals[3], the average connectome will still likely

contain relevant information about an individual's trait characteristics. Analyses and visualizations

were conducted using both MATLAB and python.

Clinical assessments

A battery of commonly used self-report questionnaires probing a wide range of clinically relevant

measures were collected immediately following the MRI scans (same day). These assessments

include the Adult Temperament Questionnaire (ATQ)[27], the Behavior Rating Inventory of

Executive Function (BRIEF)[28], the Brief Symptom Inventory (BSI)[29], the Interpersonal Reactivity

Index (IRI)[30], the Positive and Negative Affect Schedule (PANAS)[31], the Pittsburgh Sleep Quality

Index (PSQI)[32], and the Perceived Stress Scale (PSS)[33]. Two of the questionnaires (BSI and

BRIEF) provided both raw and age and sex normalized scores. In this study, we used the raw

scores for neuro-behavioral modeling to maintain consistency across clinical measures. Some

participants did not complete all clinical assessment scales. They were included in all analyses

for which they had data. A detailed breakdown of the number of subjects (*n*s) for each measure

can be found in **Supplemental Table 9**.

Cognitive assessments

A series of neuropsychological evaluations was administered by a trained evaluator to test a wide

array of cognitive functions. These were conducted in the same post-imaging session as the

clinical assessments. In total, we administered the verbal fluency, trail making, color-word

interference, and twenty questions subtests from the Delis-Kapan Executive Function Scale (D-

KEFS)[34], the letter-number sequencing, symbol search, and cancellation subtests from the

Wechsler Adult Intelligence Scales (WAIS)[35], the vocabulary and matrix reasoning subtests of the

Wechsler Abbreviated Scale of Intelligence 2nd Edition (WASI)[36], the finger windows and list

learning subtests of the Wide Range Assessment of Memory and Learning 2nd Edition

(WRAML)[37], the reading subtest of the Wide Range Achievement Test 5th Edition (WRAT)[38], and

the Boston Naming Test 2nd edition (BNT)[39]. A few of the cognitive tests provided both raw and

age and sex normalized scores. In this study, we used the raw scores for predictive modeling to

maintain consistency across all measures. Some participants did not complete all cognitive tests.

They were included in all analyses for which they had data. A detailed breakdown of the number

of subjects (*n*s) for each measure can be found in **Supplemental Table 10**.

Predictive modeling

We used CPM[3,10] to identify functional brain networks that were related to each clinical and

cognitive measure separately. Each predictive model was trained and tested in a 10-fold cross-

validation, which was repeated 1000 times to obtain a distribution of predictions. Within each

training fold, edges were selected if they were significantly correlated ($p < 0.05$) with behavior

after controlling for age and sex using partial correlations. Prediction strength was determined by

comparing the observed clinical/cognitive measures to the predicted measures using Spearman

correlations. Permutation tests were utilized for significance testing. Specifically, the number of

null prediction values that were greater than the median prediction for each measure was divided

by the number of permutations to derive the *p*-values. The *p*-values were FDR-corrected for 91

comparisons (63 clinical + 28 cognitive measures). Networks for each measure were derived by

identifying the edges that were predictive in >50% of permutations. The resulting networks were

binarized, with a '1' or '0' indicating an edge's network membership.

Assessing the effects of instruments and subdomains on prediction strength

We utilized one-way ANOVAs to assess the effect of measurement instruments and subdomains

on prediction strength for clinical and cognitive measures separately (**Fig 3a/b**). To do so,

prediction strength values from measures within the same clinical assessment subdomain or

cognitive testing battery were grouped together and compared to other subdomains/tests. The

ATQ, BRIEF, and PANAS inventories explicitly specified that the individual measures belonged

to separate subdomains (e.g., PANAS measures were split into 'positive' and 'negative' affect

domains). These separate subdomains were treated as separate categories for this analysis. The

BSI, IRI, PSQI, and PSS inventories did not specify how measures could be grouped into separate

subdomains. Therefore, all measures within these instruments were categorized as belonging to

the same subdomain for this analysis. Several of the cognitive testing batteries were composed

of sets of multiple separate cognitive tests. The D-KEFS consisted of the twenty-questions test,

the color-word interference test, the verbal fluency test, and the trail making test. Additionally, the

WASI was composed of a vocabulary test and a matrix reasoning test, the WRAML was

composed of a verbal learning test and a finger windows test, and the WAIS consisted of

cancellation, letter-number sequencing, digit-symbol coding, and symbol search tests. These

were all categorized as belonging to different subdomains for this analysis, since they were all

different cognitive tests. Conversely, all the metrics from the BNT captured various aspects of

BNT performance and were thus considered as belonging to the same subdomain.

Obtaining measurement reliability data

Test-retest reliability (ICC) measures were obtained from the original papers and/or technical and

user manuals published for each clinical and cognitive inventory. The BRIEF provided separate

ICC data from a normative sample and a mixed clinical/healthy adult population. We used the

ICC data from the mixed clinical/healthy adult sample, since it more closely matched our study's

participant population. The original paper validating the ATQ provided ICC data collected from 2

separate studies, one conducted in undergraduate students and the other in adults between 26

and 91 years old (median age = 57 years). We utilized the data from the study conducted in

undergraduate students because it provided ICC data for all the ATQ measures that we used

here, while the other study did not. Additionally, our sample's median age (31.17 years) is closer

to the median age of typical undergraduate populations. The IRI reported ICC data from males

and females separately. We averaged those results for use in the analysis here. There were no

ICC data reported for the 'total questions asked' measure from the twenty-questions subtest in

the D-KEFS, the verbal learning intrusion measure in the WRAML, or for the performance

measures on the BNT (except for 'total score'). Therefore, these measures were omitted from

analyses examining the relationship between ICC and prediction performance.

Identifying relationships between measures and calculating network similarity

Spearman correlations were calculated for each pair of measures that CPM significantly

predicted, and the derived *p*-values were FDR corrected for multiple comparisons. Network

similarity between measures was assessed using Dice similarity coefficients. If there was a

positive relationship between two measures, then the Dice coefficient was calculated between

the positively predicting network for measure A and the positively predicting network for measure

B, and then calculated once more between the negatively predicting network for measure A and

the negatively predicting network for measure B. If there was a negative relationship between two

measures, then the Dice coefficient was calculated between the positively predicting network for

measure A and the negatively predicting network for measure B, and then calculated once more

between the negatively predicting network for measure A and the positively predicting network for

measure B. A weighted average of these two Dice coefficients was taken and used to examine

overall network similarity between measures.

Comparing network similarity across measures

We sorted the measures based on network similarity in the interest of identifying meaningful

commonalities and differences between predictive networks across measures. To achieve this,

we input the inverse of this full Dice similarity matrix (i.e., Dice distances) into an agglomerative

hierarchical clustering algorithm using Ward's method. This yielded a dendrogram that sorted the

measures based on their predictive networks' similarities. The measures were grouped into

clusters based on the hierarchical clustering results. The number of clusters chosen was

determined using the elbow method[42], which evaluates where the incremental decrease in within-

cluster sum of squares (WCSS) begins to slow across increasing values of k. The point of

maximum curvature (i.e., the "elbow") was objectively identified using the KneeLocator

algorithm[77]. This is a commonly used approach for determining an appropriate number of clusters

in a dataset. However, we performed clustering with the intention of reducing dimensionality,

showing how the measures grouped based on network similarity, and to compare important

features driving CPM predictions across measures, rather than to make any claims about how

many clusters exist in this dataset.

To identify the extent to which the same nodes were important to positively and negatively

predicting clinical and cognitive measures, we calculated the Jaccard similarity between vectors

representing the top 10% highest degree nodes in the positive and negative predictive networks

for each cluster. Overlap was summarized as the mean of the pairwise Jaccard values, and one-

sided permutation tests (10,000 iterations) were utilized for significance testing. The *p*-values

were calculated as the proportion of null replicates that exceeded the observed mean Jaccard

similarity.

Identifying localizations of predictive networks

The binarized positively and negatively predicting networks for measures within a cluster were

summed separately and Z-scored. This yielded aggregate positively and negatively predicting

networks for each cluster, with edges most important to predictions across measures weighted

most heavily. Before summing the networks, we ensured that the directionality of all the measures

within a cluster was similar so that networks positively related to symptoms or cognition would not

be mistakenly combined with networks negatively related to symptoms or cognitions. For

example, if there was one measure in a cluster where a higher score was desirable while lower

scores were desirable for the remaining measures, then the positive network for the first measure

would be summed with the negative networks for the other measures (and vice versa). The

distribution of edges within and between canonical networks was evaluated by summing the

edges within each canonical network pair from the aggregated cluster networks. We utilized the

Yeo17 networks[43] as network definitions, plus the cerebellum, brainstem, and subcortical regions.

The nodes important to predictions were examined by calculating degree centrality for each node.

The degree values were then projected onto the FreeSurfer template brain's ('fsaverage') pial

surface, along with cerebellar and brainstem surface reconstructions rendered in Bioimage Suite.

These degree plots were created using Python's nilearn package[78].

Network mediators of relationships between clinical and cognitive measures

For each pair of significantly correlated clinical-cognitive measures, we computed the shared

network connectivity by identifying and summing the edges that were predictive for both

measures. If the correlation between a pair of clinical-cognitive measures was positive, then the

shared network connectivity was defined as the sum of the positively predicting edges shared by

both measures minus the sum of negatively predicting edges shared by both measures.

Conversely, if the correlation between the measures was negative, then the shared network

connectivity was defined as the sum of edges that were positively predicting for one measure but

negatively predicting for the other minus the sum of edges that were negative predicting for the

first measure but positively predicting for the other. Causal mediation analyses were conducted

using Python's pingouin package[79] to test whether the shared network connectivity mediated

relationships between clinical and cognitive measures. Path coefficients were estimated with

ordinary least squares regression, and the indirect effect was evaluated using 1,000 bootstrap

resamples with a two-tailed $\alpha = 0.01$. Significance was determined by whether the 99% bootstrap

confidence interval excluded zero. The mediation analyses were conducted bidirectionally for all

pairs of significantly correlated clinical-cognitive relationships, and since we did not have any

hypotheses on the directionality of the mediations, we reported the larger of the two indirect

mediation coefficients.

The nodes important to mediating these relationships were examined by 1) deriving binarized

matrices for each pair of significantly correlated clinical-cognitive measure pairs that indicated

whether each edge was predictive in both measures, 2) summing these matrices across all significantly correlated clinical-cognitive measure pairs within each clinical-cognitive cluster, 3) Z-scoring this summed matrix, and 4) calculating the degree centrality for each node. The degree centrality of the summed shared networks for all significantly correlated clinical-cognitive measure pairs within each clinical-cognitive cluster was visualized on the brain surface the same way as before using Python's nilearn package[78].

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Code availability

The code used in all of the main analyses conducted in this study can be found at: https://github.com/YaleMRRC/TDS_measure_predictions_and_mediations.git. All dependency files required to run this code are also provided in this GitHub repository (e.g., cortical surface files), as is the relevant input data.

Competing interests

G.S. has served as a consultant or scientific advisory board member to Axsome Therapeutics, Biogen, Biohaven Pharmaceuticals, Boehringer Ingelheim International, Bristol-Myers Squibb, Clexio, Cowen, Denovo Biopharma, ECR1, EMA Wellness, Engrail Therapeutics, Gilgamesh, Janssen, Levo, Lundbeck, Merck, Navitor Pharmaceuticals, Neurocrine, Novartis, Noven Pharmaceuticals, Perception Neuroscience, Praxis Therapeutics, Sage Pharmaceuticals, Seelos

Pharmaceuticals, Vistagen Therapeutics and XW Labs; and received research contracts from

Johnson & Johnson (Janssen), Merck and Usona. G.S. holds equity in Biohaven Pharmaceuticals

and is a co-inventor on a US patent (8,778,979) held by Yale University and a co-inventor on US

provisional patent application no. 047162-7177P1 (00754), filed on 20 August 2018 by Yale

University Office of Cooperative Research. Yale University has a financial relationship with

Janssen Pharmaceuticals and may receive financial benefits from this relationship. The University

has put multiple measures in place to mitigate this institutional conflict of interest. Questions about

the details of these measures should be directed to Yale University's Conflict of Interest office.

V.H.S. has served as a scientific advisory board member to Takeda and Janssen. The remaining

authors declare no competing interests.

Figure 1. Prediction strength of clinical measures. The boxplots on the right show the prediction strength of each measure and are colored green if significantly predicted by CPM (*pFDR* < 0.05). Measures are grouped according to the instrument they belong to, as indicated by the encircled bolded acronym to the left of the outermost brackets, and the solid horizontal black lines between the boxplots. Measures within instruments were grouped into subdomains if applicable, which are indicated by the middle-level of brackets and the dashed black lines between the boxplots.

Figure 2. Prediction strength of cognitive measures. The boxplots on the right show the prediction strength of each measure and are colored purple if significantly predicted by CPM ($pFDR < 0.05$). Measures are grouped according to the testing battery they belong to, as indicated by the encircled bolded instrument acronym to the left of the outermost brackets, and the solid horizontal black lines between the boxplots. Measures within the D-KEFS were further subdivided because this battery was composed of subtests that each yielded multiple performance metrics. This is indicated by the middle-level of brackets and the dashed black lines between the boxplots.

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Figure 3. **Prediction strength was driven by phenotype measured. A)** Clinical predictions
varied significantly by instrument and subdomain (one way ANOVA: $p < 0.001$). **B)** Cognitive
predictions varied significantly by tests and subtests (one way ANOVA: $p < 0.001$). Prediction
strength was unrelated to other measurement characteristics, such as test-retest reliability (ICC)
(top), skewness (middle), and variance (top) for clinical (panel **C**) and cognitive measures (panel
D).

Figure 4. Relationships between measures. The measures' predictive networks were sorted according to their Dice similarities by an agglomerative hierarchical clustering algorithm (upper triangle). A dendrogram displayed above the matrix highlights how the measures grouped together based on their network similarity. Descriptive labels were given to the 9 clusters and displayed underneath the dendrogram. The measures belonging to each cluster were surrounded black borders on the matrix and colored differently on the dendrogram. The clinical measures were displayed on the top/left and the cognitive measures were displayed on the bottom/right. The network similarity was mirrored by the correlational structure between the raw measures (lower triangle).

Figure 5. Brain networks driving predictions. A) The clusters summarizing networks important to predicting clinical measures are displayed with the descriptive labels 'psychiatric symptoms', 'executive functioning', 'sleep', 'distress', and 'positive affect'. **B)** The clusters summarizing networks important to predicting cognitive measures are displayed with the descriptive labels

'lexical retrieval', 'cognitive control', 'fluid intelligence, and 'verbal fluency'. For each cluster,
degree plots highlight the important nodes for predictions across all measures, and matrices
highlight the distribution of edges connecting canonical networks. Networks are labeled according
to the Yeo 17 network definition, plus cerebellar, subcortical, and brainstem regions.

Figure 6. Shared networks mediate clinical-cognitive relationships. A) An overview of how
the shared networks were identified and how mediation analyses were conducted for significantly
correlated pairs of clinical and cognitive measures. Predictive networks for each measure in a
correlated pair were compared, and edges that were predictive for both measures were summed.
This sum was used as a mediating variable to test whether the shared network connectivity
mediated the relationships between the correlated clinical and cognitive measure pairs. This was
repeated for every pair of significantly correlated pair of clinical and cognitive measures (*pFDR* <
0.05). **B)** This matrix displays the indirect mediation coefficients for all the significantly correlated
clinical-cognitive measure pairs. The shared network connectivity significantly mediated every
pair of significant clinical-cognitive correlations. Measures were grouped by their cluster
assignment in the visualization. **C)** Average degree centrality for the mediating networks across
all clinical-cognitive measures within all possible pairs of clusters were computed and projected
onto cortical surfaces to highlight the regions important for mediating clinical-cognitive
relationships within cluster pairs.

Figure 7. Networks important to generally mediating clinical-cognitive relationships. Average degree centrality for all mediating networks was computed and projected onto a cortical surface to highlight the regions important for generally mediating clinical-cognitive relationships (left). The surface plot was thresholded to display the top 10% most important nodes for mediations. The matrix on the right highlights the distribution of edges connecting canonical networks. The matrix was thresholded to only display the top 10% most important canonical network-network connections for mediations. Networks were labeled according to the Yeo 17 network definition, plus cerebellar, subcortical, and brainstem regions.

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