Title: Astrocytic PIEZO activation by heartbeat sound promotes extracellular matrix and maturation in human brain organoids

Short title: Heartbeat promotes ECM via PIEZO

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Abstract:

Heartbeat sound is one of the first rhythmic stimuli encountered by the developing human brain, yet its biological role has remained unexplored. Here we show that heartbeat sound promotes structural and functional maturation of human cortical organoids with a physiological astrocyte-to-neuron ratio. Continuous stimulation with heartbeat expanded the extracellular space (ECS), visualized by super-resolution 3D STED and 2-photon shadow imaging, and increased extracellular matrix (ECM) synthesis, detected by LC-MS/MS proteomics. Heartbeat sound promoted neuronal and astrocytic differentiation, synaptogenesis, and organoid maturation, as shown by single-cell RNA sequencing, synaptic marker immunohistochemistry, and high-density multielectrode electrophysiology. Transcriptomic analyses demonstrated astrocyte-specific expression of mechanosensitive PIEZO channels. Using Ca^{2+} imaging, we confirmed that low-frequency sound stimulation, including heartbeat, activates PIEZO-mediated Ca^{2+} responses, which in turn upregulate astrocytic ECM synthesis. Experiments with biomimetic hydrogels demonstrated that physiological matrix stiffness attenuates PIEZO activation, suggesting a mechanoprotective mechanism. Our findings demonstrate a fundamental mechanism for inducing ECM synthesis and neural differentiation through astrocytic PIEZO activation by heartbeat sound, suggesting that interoception of the internal acoustic environment is an underappreciated driver of human brain development.

Keywords: mechanoreceptor, neuron-glia interactions, extracellular matrix, extracellular space, cortical organoid, neurodevelopment

Highlights

- Heartbeat sound activates PIEZO ion channels
- Astrocytic PIEZO activation promotes extracellular matrix synthesis
- Heartbeat sound stimulates neural differentiation and brain organoid maturation

63 **Graphical Abstract**

Introduction

Mother's heartbeat is one of the first sounds that a human fetus hears starting the third trimester of pregnancy (Querleu et al., 1988). Yet, even before the auditory system fully develops, the embryo is exposed to acoustic stimulation, which is dominated by sound frequencies below 200 Hz including those elicited by maternal heartbeat (Dealessandri and Vivalda, 2018; Vince et al., 1982). While the high frequencies are strongly attenuated inside the womb, low frequency sounds can be as loud as 100 dB (Dealessandri and Vivalda, 2018; Gerhardt et al., 1990). Therefore, the acoustic environment of an embryo is defined by low-frequency sound waves generating persistent mechanical oscillations that rhythmically stimulate developing tissues.

In mammalian tissues, mechanical oscillations are mainly detected by PIEZO ion channels (Coste et al., 2010; Zhao et al., 2018), which have been implicated in interoceptive regulation of breathing (Tort et al., 2025) and blood pressure (Jammal Salameh et al., 2024; Zeng et al., 2018). PIEZO1 and PIEZO2 are mechanically activated ion channels that share a common activation mechanism gated by membrane tension. While PIEZO2 is predominantly expressed by somatosensory neurons, PIEZO1 is also found in glial (Chi et al., 2022), vascular (Ranade et al., 2014), and immune cells (Solis et al., 2019).

The molecular mechanisms of sound-driven mechanotransduction remain underinvestigated. Although the possibility of inducing cellular responses by sound stimulation has been demonstrated (Kumeta et al., 2025; Xu et al., 2024), the physiological relevance and mechanistic understanding of such stimulation has remained elusive. We hypothesized that heartbeat sound provides a natural mechanical stimulus that shapes embryonic brain development.

For experimental studies of human neurodevelopment, brain organoids derived from human induced pluripotent stem cells (hiPSCs) have become the model of choice. Originally designed to recapitulate cortical organization (Lancaster et al., 2013) and to model developmental disorders, organoid systems have since been adapted to study interactions between brain regions and to investigate connectivity-related diseases such as epilepsy (Onesto et al., 2024). Despite these advances, current organoid models do not capture the acoustic environment during early brain development. In this study, we investigated how mechanostimulation with heartbeat sound shapes cellular physiology and functional maturation in human cortical organoids, focusing on the brain extracellular matrix (ECM), neural cell differentiation, synaptogenesis, and neuronal activity.

Results

Heartbeat sound expands the extracellular space in astrocyte-enriched organoids

Astrocyte-enriched cortical organoids were generated by co-culturing neural precursor cells (NPCs) with induced astrocytes (iAstrocytes) using a modified growth factor-based protocol (Paşca et al., 2015) (**Fig. 1A**). By day 45, they developed ramified astrocytes, glutamatergic synapses, and showed increased ECM expression compared with non-enriched cortical organoids (**Fig. S1**). Cortical organoids with and without astrocyte enrichment were exposed to a human heartbeat audio recording for 31 days of maturation, with ambient noise as control. Hydrophone measurements in cultivation medium (**Fig. 1B**) were used to tune the applied heartbeat sound to physiological acoustic environment of an embryo during gestation (**Table 1**).

Heartbeat sound increased the extracellular space (ECS) volume fraction in astrocyte-enriched organoids by 39% (23.4±3.5 vs 16.8±6.2 %, mean±SD) (**Fig. 1C, C'**), shown by 3D STED superresolution shadow imaging (SuSHi) (Tonnesen et al., 2018), explained in (**Fig. S2**). This observation was confirmed with 2-photon shadow imaging indicating a 31% (33.1±5.6 vs 25.2±5.8 %, mean±SD) ECS volume increase in astrocyte-enriched organoids stimulated with heartbeat sound (**Fig. 1D, D'**). Higher ECS volume fractions measured with 2P are due to lower resolution compared with 3D STED (**Table S1**) and consequent under-detection of small cellular structures. No major changes in the ECS volume were observed in organoids without astrocyte enrichment (**Fig. S3**).

Heartbeat sound promotes ECM synthesis in astrocyte-enriched organoids

Because the expanded ECS needs to be stabilized by an extracellular scaffold to maintain tissue integrity and diffusion (Tønnesen et al., 2023), we next analyzed protein expression using LC-MS/MS. Gene Ontology Cellular Component (GOCC) enrichment analysis comparing heartbeat-stimulated and control organoids revealed ECM among the top regulated terms (**Fig. 1E**). In astrocyte-enriched organoids, heartbeat sound stimulation upregulated multiple ECM scaffolding proteins, among them fibronectin (FN1) and vitronectin (VTN), and synapse organizing molecules including glypican 4 (GPC4), neuroligins (NLGN1, NLGN2), and plexin-B (PLXNB1) (**Fig. 1F** and **Fig. S4**). In organoids without astrocyte enrichment, we found no major changes in ECM expression following heartbeat sound stimulation (**Fig. S4**).

Figure 1. Stimulation with heartbeat sound increases ECS volume and ECM expression in astrocyte-
enriched human cortical organoids. (**A**) Generation of organoids and exposure to heartbeat. (**B**)
Hydrophone recording and power spectrum of the applied heartbeat sound in cultivation medium. (**C**)
Superresolution 3D STED shadow imaging and ECS segmentation (red) in live organoids. (**C'**) ECS volume
fraction comparison, t-test (n=10-15). (**D**) 2-photon shadow imaging and ECS segmentation (red) in live

organoids. (**D'**) ECS volume fraction comparison, t-test (n=5-6). (**C**, **D**) Images are xy and zy projections;
LUT inverted (see **Fig S2** for details). Scale bars, 50 µm. (**E**) Gene ontology cellular component (GOCC)
enrichment analysis of protein expression in heartbeat-stimulated vs control astrocyte-enriched organoids,
based on significantly regulated proteins (p < 0.05, fold change difference > 1.5, t-test), measured by LC-
MS/MS. (**F**) Heatmap shows normalized, centered (mean subtraction) log2 protein abundances of selected
ECM proteins regulated by heartbeat sound. Other regulated ECM proteins are shown in **Fig S4**.

Heartbeat sound promotes neural differentiation in astrocyte-enriched organoids

The brain ECM is jointly produced by neurons and glial cells, forming a dynamic scaffold
that controls cell differentiation and neuroplasticity (Dzyubenko and Hermann, 2023; Faissner and
Reinhard, 2015). To examine cellular composition and phenotypic changes induced by heartbeat
sound, we performed single-cell RNA sequencing (scRNAseq). In astrocyte-enriched organoids,
heartbeat sound stimulation increased glutamatergic neuron differentiation (23.7 % vs 13.5 % of
total cell counts, heartbeat vs control) (**Fig. 2A**), while no significant cell composition changes
were observed in non-enriched organoids (**Fig. S5A**).

A deeper analysis of astrocytic subpopulations by unsupervised clustering (**Fig. S6** and
Supplementary Table 2) revealed 11 distinct phenotypes (**Fig. 2B**) in astrocyte-enriched and 6
phenotypes in non-enriched organoids. Among the 11 phenotypes in astrocyte-enriched
organoids, heartbeat sound stimulation promoted the cluster of neurotrophic and synaptogenic
astrocytes (28.5 % vs 16.1 % of astrocyte cell counts, heartbeat vs control). Organoids without
astrocyte enrichment showed no major changes in astrocytic subpopulations (**Fig. S5B**).

Heartbeat promotes synaptogenesis and activity in astrocyte-enriched organoids

Synaptogenic astrocyte differentiation revealed by scRNAseq was further supported by
the upregulation of synaptic proteins detected by LC-MS/MS proteomics. Among the 137
synapse-associated proteins that were upregulated by heartbeat sound stimulation in astrocyte-
enriched organoids (**Fig. S7**), we found multiple synaptic adhesion molecules and astrocyte-
derived synapse maturation factors including Glypican 4 (GPC4).

Synaptic marker immunolabelling confirmed the increased synaptogenesis in astrocyte-
enriched organoids following heartbeat sound stimulation (**Fig. 2C, C'**). Quantifications of
postsynaptic puncta containing glutamate receptor subunit 1 (GLUA1), presynaptic vesicular
glutamate transporter 1 (VGLUT1), and their overlaps indicated the formation of complete
synapses. In cortical organoids without astrocyte enrichment, heartbeat stimulated GLUA1
clustering but not complete synapse formation (**Fig. S8**).

Moreover, high-density multielectrode array (HD-MEA) recordings showed significantly
higher spontaneous neuronal activity in heartbeat-stimulated astrocyte-enriched organoids (**Fig.
2D, D'**). While the non-stimulated organoids exhibited little to no spontaneous electrical activity

after 31 days of maturation, in agreement with previous reports (Alam El Din et al., 2025; Trujillo

et al., 2019), the heartbeat-stimulated organoids demonstrated significantly higher proportion of

active units and increased mean firing rates. These results indicate that stimulation with heartbeat

sound promotes functional maturation in astrocyte-enriched organoids.

Figure 2. Stimulation with heartbeat sound promotes neural differentiation, synaptogenesis, and

spontaneous activity.

(**A**) Transcriptomic UMAP map generated from scRNAseq data shows key cellular lineages in astrocyte-

enriched organoids. Cell type percentages are shown as stacked bar charts. (**B**) Astrocyte subtypes

revealed by cluster analysis of astrocytic transcriptomes (see **Fig. S6** and **Supplementary Table 2** for

functional interpretation). Astrocyte subtype percentages are shown as stacked bar charts. (**C**)

Immunohistochemical analysis of synaptic markers VGLUT1 (cyan) and AMPA receptor subunit GLUA1

(yellow). Neuronal dendrites are labeled with MAP2 (magenta), and nuclei (blue) are counterstained with

DAPI. Scale bar, 50 µm. (**C'**) Quantifications of GLUA1, VGLUT1 synaptic puncta, and their overlaps. (n=9).

(**D**) Spontaneous neuronal activity in astrocyte-enriched organoids is shown by high-density multi-electrode
array (HD-MEA) activity maps. Scale bar, 500 μm. (**D'**) Quantifications of active units and their mean firing
rates (n=3-4). (**C', D'**) Statistical significance was assessed by unpaired two-tailed t-tests.

Heartbeat sound stimulates astrocytic PIEZO receptors

Because sound waves propagate as mechanical deformations in a medium, we
hypothesized that the observed effects of heartbeat sound stimulation on organoid maturation
can be mediated by mechanoreceptors. scRNAseq data demonstrated that mechanosensitive
PIEZO1 and PIEZO2 ion channels (Coste et al., 2010) are selectively expressed by astrocytes
and dividing cells (**Fig. 3A**). Because dividing cells are a minor cell population (comprising < 2 %
of total cells), we further investigated mechanotransduction of heartbeat sound in astrocytes.

To perform simultaneous acoustic stimulation with heartbeat-like sound and Ca^{2+} imaging,
we used a custom-built device (**Fig. S9**), adapted from (Kumeta et al., 2025). Ca^{2+} imaging in
maturated iAstrocytes revealed robust responses to both short (20 s) heartbeat sound stimulation
(**Table 1**) and bath application of selective PIEZO1 agonist Yoda1 (Evans et al., 2018) (**Fig. 3B,**
C). Notably, the undifferentiated NPCs showed only minimally detectable responses to both
heartbeat sound and Yoda1, indicating that the heartbeat sensitivity is a feature of maturating
astrocytes (**Fig. S10**).

To test whether heartbeat-like sound stimulation selectively activates PIEZO1
mechanosensitive ion channels, we performed Ca^{2+} imaging in a human embryonic kidney
(HEK293) cell model lacking endogenous PIEZO1 expression (HEK293-P1KO) (Dubin et al.,
2017). PIEZO1 expression was induced using a plasmid vector with a fluorescent reporter
mScarlet to identify transfected cells (**Fig. 3D**). Both short (20 s) stimulation with heartbeat sound
and bath application of Yoda1 elicited sustained Ca^{2+} increase in PIEZO1-expressing cells,
whereas mock-transfected controls remained inactive (**Fig. 3E**). Notably, co-application of
heartbeat stimulation with a non-activating Yoda1 concentration (0,01 μM; IC_{50} in HEK cells ~1.3
μM) amplified the Ca^{2+} response, while controls remained silent, confirming the specificity of
PIEZO1 activation by heartbeat sound (**Fig. S11**).

PIEZO1 activation triggers ECM expression in mouse astrocytes

To investigate the downstream effects of astrocytic PIEZO activation by low-frequency
sound stimulation, we applied short 1 s sound bursts with a dominant frequency of 150 Hz (**Fig.**
S12A) in primary mouse astrocytes. This mode of PIEZO1 activation evoked similar responses
as human heartbeat sound stimulation in HEK cells (**Fig. S12B**). In mouse astrocytes, short sound
bursts evoked more robust responses than human heartbeat sound (**Fig. 4A**, **B** and **Fig. S12C-**
F), making this PIEZO1 activation regime preferable for downstream signaling studies.

Figure 3. Astrocytic PIEZO ion channels mediate calcium responses evoked by heartbeat.
(**A**) Dot plots generated from scRNAseq data show cell-specific expression of mechanosensitive PIEZO channels in astrocyte-enriched organoids. (**B**) Time-lapse t-projection and fluorescence intensity profiles show heartbeat sound-evoked Ca^{2+} responses in human iAstrocytes at 28 days of maturation. Scale bar, 50 µm. (**C**) Averaged Ca^{2+} responses evoked in iAstrocytes (magenta) by heartbeat sound stimulation and 10 µM Yoda1 application (20-25 cells, n=6). (**D** HEK293-P1KO cells were co-transfected with the GCaMP6f Ca^{2+} indicator and PIEZO1-mScarlet or Mock vectors. (**E**) Averaged Ca^{2+} responses evoked by heartbeat sound stimulation and 10 µM Yoda1 application in HEK cells with (red) and without (blue) PIEZO1 (23-39 cells, n=5). Scale bars, 50 µm.

To reveal protein expression changes induced by astrocytic PIEZO1 activation, we performed LC-MS/MS proteomics following a 3-hour incubation with 10 µM Yoda1 combined with ten acoustic bursts delivered during the first 10 minutes (**Fig. 4C**). Thereby induced astrocytic PIEZO1 activation increased the expression of ECM scaffolding components including the network-forming collagen COL8A1, pentraxin PTX3, ECM-remodeling enzymes including matrix metalloproteinases with thrombospondin motifs ADAMTS1 and ADAMTS8, and ECM-crosslinking

232   transglutaminase TGM1 (**Fig. 4C** and <u>Fig. S13A</u>). Intracellularly, PIEZO1 activation induced Ca^{2+}

233   response and inflammation-associated transcriptional factor expression (<u>Fig. S13B</u>).

Biomimetic ECM hydrogels attenuate PIEZO1 activation by low-frequency sound

Because the extended activation of PIEZO1 in mouse astrocytes stimulated stress-

associated pathways, we hypothesized that the brain ECM can modulate cellular responses to

mechanical stimulation such as low-frequency sound. To test this hypothesis, we covered the

GCaMP6f-expressing primary mouse astrocytes with ECM-mimetic hydrogels with tunable

stiffness corresponding to soft and physiologically stiff brain ECM (**Fig. 4D**). Under 150 Hz sound

burst stimulation, the hydrogels significantly attenuated PIEZO activation, indicated by decreased

amplitude of Ca^{2+} responses and reduced fraction of responding astrocytes.

Figure 4. PIEZO1 activation and its downstream signaling in primary mouse astrocytes.

(**A**) Time-lapse t-projection and fluorescence intensity profiles show heartbeat-evoked Ca^{2+} responses in
mouse primary astrocytes. Scale bar, 50 μm. (**B**) Averaged Ca^{2+} responses evoked in astrocytes by low-
frequency sound bursts and 10 μM Yoda1. (38-42 cells, n=8). (**C**) LC-MS/MS measurements were
performed 3 hours after PIEZO1 activation in mouse astrocytes. Volcano plot shows key ECM protein
regulations induced by PIEZO1 activation, compared versus control. (n=5). For a full list of regulated
proteins see **Fig. S13**. (**D**) Ca^{2+} responses to low-frequency sound bursts are quantified in astrocytes
covered with biomimetic ECM hydrogels with variable stiffness. (n=4). Intergroup differences were analyzed
by one-way ANOVA followed by t-tests.

DISCUSSION

Our findings demonstrate a novel mechanism for activating ECM synthesis and neural
differentiation via mechanotransduction of physiological sound stimuli. Heartbeat sound
stimulation of astrocytic PIEZO ion channels promoted the differentiation of neurotrophic
astrocytes and glutamatergic neurons. Neural cell differentiation was accompanied by
coordinated expansion of ECS and ECM synthesis, which supported functional neuronal
maturation in human cortical organoids. This evidence suggests interoception of the internal
acoustic environment as an underappreciated driver of human brain development.

We show that the neurodevelopment and maturation promoting effects of heartbeat sound
stimulation in human brain organoids are astrocyte dependent. Heartbeat sound induced ECM
synthesis, neural differentiation, synapse formation, and spontaneous neuronal activity
exclusively in the astrocyte-enriched organoids. These findings align with the established role of
astrocytes in ECM remodeling and regulation of neuroplasticity (Dzyubenko and Hermann, 2023).
Consistent with the function of PIEZO ion channels in mouse hippocampal neurogenesis (Chi et
al., 2022), we found that activation of astrocytic PIEZO channels by heartbeat sound promoted a
neurotrophic and synaptogenic astrocyte phenotype. Given that our scRNAseq data
demonstrated predominant PIEZO expression in astrocytic lineages, these results suggest that
astrocytes are key interoceptors sensing and transducing internal acoustic stimuli during human
neurodevelopment.

This finding was enabled by our astrocyte enrichment protocol, which achieves a
physiological 1:1 astrocyte-to-neuron ratio (von Bartheld et al., 2016). Delayed astrocytic
differentiation and maturation in conventional human cortical organoids (Sloan et al., 2017) is a
limitation for investigating astrocyte-mediated mechanisms. Our approach supports the early
emergence of mature, ramified astrocytes. Furthermore, single-cell transcriptomics revealed
diverse astrocyte subtypes including perisynaptic and regulatory phenotypes, establishing this
model as a powerful tool for investigating astrocyte-neuronal interactions and their contributions
to human cortical development.

We demonstrate that PIEZO channels are activated by low-frequency sound stimulation
resembling the acoustic environment *in utero* (Gerhardt et al., 1990; Vince et al., 1982). While
brief 150 Hz sound bursts elicited transient PIEZO activation, rhythmic heartbeat sound with the
dominant frequency of 100 Hz induced sustained intracellular Ca^{2+} elevations. Continuous
stimulation with alternating pressure beyond 10 Hz has been shown to rapidly deactivate PIEZO1
(Lewis et al., 2017). However, that effect was observed during prolonged sinusoidal stimulation
for 4 seconds, whereas the individual heartbeat pulses used here did not exceed 0.15 seconds,
verified by hydrophone recordings. Consistent with previous studies showing neuronal activation
in response to repetitive mechanostimulation *in vitro* (Nikolaev et al., 2015) and *in vivo* (Jammal
Salameh et al., 2024), we demonstrate that rhythmic heartbeat sound and consecutive sound
bursts robustly activate mechanotransduction in astrocytes. Together with proteomic evidence for
upregulated Ca^{2+} responsive transcriptional factors and ECM expression, these data indicate that
PIEZO activation by heartbeat induces Ca^{2+}-dependent ECM synthesis in astrocytes.

Astrocyte-dependent ECM synthesis and ECS expansion facilitated functional maturation
of heartbeat-stimulated human brain organoids. While the ECS provides the diffusion routes for
ions and metabolites essential for neuronal activity (Sykova and Nicholson, 2008), uncontrolled
ECS enlargement can create "dead-space" microdomains that impair rather than facilitate
diffusion and signaling (Hrabetová et al., 2003). Stabilization by ECM is therefore crucial, with the
core scaffolding components providing a macromolecular network that binds regulatory molecules
(Fawcett et al., 2022), mediates neuron-glia interactions (Dzyubenko and Hermann, 2023), and
controls neuronal plasticity (Dityatev et al., 2010). Thus, the coordinated increase in ECM
synthesis and ECS volume established a homeostatic environment that supported glutamatergic
neuron differentiation, synapse formation, and neuronal activity following heartbeat sound
stimulation in astrocyte-enriched cortical organoids.

In addition to the maturation-associated benefits of astrocytic mechanostimulation, a
prolonged PIEZO activation also induced inflammatory signaling. In this context, our experiments
with biomimetic hydrogels indicate a mechanoprotective role of the brain ECM. By attenuating
PIEZO activation, physiologically stiff ECM buffers astrocytic responses to mechanical
stimulation. This dual role of facilitating supportive signaling while preventing excessive activation
suggests ECM is a homeostatic regulator of mechanotransduction in the developing brain.

Our findings open an intriguing direction for developing ECM-promoting therapies in
multiple neurological disorders that are associated with ECM degradation, including stroke
(Dzyubenko et al., 2023) and Alzheimer's disease (Crapser et al., 2020). Strategies to restore
ECM, particularly neuron-supportive components, remain elusive. We show that these

components can be stimulated by low-frequency sound through astrocytic PIEZO activation.
While focused ultrasound has been explored for neuromodulation (Kosnoff et al., 2024), its clinical
translation has been limited by uncertain mechanisms. By revealing how astrocytes respond to
low-frequency sound, this work suggests a promising approach for harnessing astrocyte-
mediated ECM remodeling for neurological recovery.

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METHODS

EXPERIMENTAL MODEL

Human cortical organoids and induced astrocytes

Neural progenitor cells (NPCs) were differentiated from a highly characterized female
control human induced pluripotent stem cell line (SCTi003-A). hIPSCs were plated onto low-
adherence AggreWell 800 plates in STEMdiff SMADi neural induction medium and 10µM of Y-
27632. During the next 5 days, half of the medium was replaced daily. On day 6, embryonic bodies
were replated on a Matrigel coated 6-well plates and full-medium changes were performed daily.
On day 12, neural rosette selection was performed using STEMdiff Neural Rosette Selection
Reagent for 1,5 hours. After re-plating, daily full-medium changes were performed until the cells
formed a monolayer and were ready for passaging. The resulting NPCs can be maintained further
with STEMdiff neural progenitor medium.

For quality control and as a shortcut in time-sensitive experiments, ready-to-use NPCs
differentiated from the same hIPSC control line (SCTi003-A) were used. Before further
differentiation, NPCs were expanded on Matrigel coated 6 well plates in STEMdiff neural
progenitor medium, during a maximum of 3 passages, using Accutase enzymatic solution for cell
dissociation. NPC cell bank was regularly checked upon each passage for characteristic
morphology and marker expression as SOX2 and Nestin, and the absence of OCT4 by
immunofluorescence.

Human induced astrocytes (iAstrocytes) were differentiated from NPCs for 3 weeks using
STEMdiff astrocyte differentiation medium and maturated using serum-free STEMdif astrocyte
maturation medium. iAstrocytes were grown on Matrigel-coated 6-well plates and passaged
weekly using Accutase.

For generating human cortical organoids, NPCs were dissociated with Accutase and
plated on low-adherence AggreWell 800 plates at 0.2×10^6 cells/well. To generate astrocyte-
enriched organoids, iAstrocytes at 1 week of maturation were co-seeded together with the NPCs
at a 2:1 ratio. Cortical organoid differentiation and maturation was achieved as described by (Birey
et al., 2017), with minor modifications. In brief, cortical differentiation was induced using the
STEMdiff dorsal forebrain organoid expansion medium containing 20 ng/ml EGF and 20 ng/ml
FGF2. After 14 days of differentiation, medium was replaced with the STEMdiff dorsal forebrain
organoid differentiation medium containing 20 ng/ml BDNF and 20 ng/ml NT3 for additional 21
days. During these first 35 days, medium was replaced every 2 days. For further maturation, the
organoids were maintained in STEMdiff neural organoid maintenance medium without

differentiation factors. For analysis, the organoids were transferred to imaging dishes at D45 (31

days of maturation).

HEK293 cells with PIEZO1 knockout (HEK293-P1KO)

366   HEK293 cells lacking PIEZO1 (HEK293-P1KO) were maintained under standard cultivation

367   conditions in DMEM containing 25 mM glucose, 10% fetal bovine serum, and 1% penicillin-

368   streptomycin. The HEK293-P1KO cell line was kindly provided by Ardem Patapoutian's laboratory

369   (Dubin et al., 2017).

Primary mouse astrocytes

Mouse astrocyte cultures were prepared from early postnatal Ai95D (Rosa-CAG-LSL-

GCaMP6f) mice as described previously (Borbor et al., 2023; Gottschling et al., 2016).

Experimental procedures were approved by the local government (Landesamt für Natur, Umwelt

und Verbraucherschutz, Recklinghausen) and conducted according to the European Union

directive 2010/63/EU and local institutional guidelines. Ai95D mice were kept in groups of 3-5

animals per cage with inverse 12 h light-dark cycle and *ad libitum* access to food and water.

Cortical mixed glial cultures were obtained from newborn (P1) male and female Ai95 mice.

Astrocytic monolayers were purified by cultivation in a selective medium (DMEM with 25 mM

glucose, 10% fetal bovine serum, and 1% penicillin-streptomycin) for 7 days. Non-astrocytic cells

were removed by shaking (2 hours on a rotary shaker, 150 rpm) and 20 µM cytosine-1-β-D-

arabinofuranoside (AraC) application for 24 hours. Purified astrocytes were sub-cultivated in the

defined maintenance medium (Neurobasal supplemented with 2% B27, 1 mM L-glutamine, and

1% penicillin-streptomycin) on glass-bottom imaging dishes (µ-Dish 35 mm #81156, Ibidi,

Gräfelfing, Germany) pre-coated with 1 mg/ml poly-D-lysine at 1*10^5 cells per dish density.

For inducing Gcamp6f expression, astrocytic monolayers were incubated with 5 µM of

cell-permeant nuclei-targeted TAT-Cre recombinase enzyme (#SCR508, MilliporeSigma,

Burlington, USA) in standard cultivation medium for 7 days before sub-cultivation on imaging

dishes, as described in (Dzyubenko et al., 2021).

METHOD DETAILS

Acoustic stimulation and hydrophone recordings

391   For long-term stimulation with recorded human 70 beats per minute heartbeat (**Audio File**

392   **1**), culture dishes with organoids were maintained on top of continuously emitting (file played in a

393   loop) loudspeaker (Flatpanel CT-17803, ChiliTec) mounted inside of the cell culture incubator and

394   connected to a HiFi digital amplifier and MP3 player (Flatpanel CT-17803, sikkeby). Heartbeat

sound levels were adjusted to physiological sound levels (**Table 1**) using the precision hydrophone (8103, HBK) measurements in cell culture medium.

For short-term acoustic stimulation during calcium imaging, 20 seconds of heartbeat (**Audio File 1**) or 1 s sound burst (**Audio File 2**) was played using a custom-made direct stimulation device (**Fig. 4B**) constructed similar to (Kumeta et al., 2025). In brief, a miniature loudspeaker (8 Ohm, 1 Watt) was attached to the lid of an imaging dish used for confocal microscopy. To achieve the direct transfer of acoustic waves produced by the loudspeaker, a coupler (the red cap of a 15 ml falcon tube) was glued to the loudspeaker membrane. The recorded sound files (**Audio File 1** or **Audio File 2**) were played via an MP3 player using the trigger after the baseline calcium measurements were performed. Sound pressure levels were adjusted close to maximal sound pressure levels *in utero* using the hydrophone.

Table 1. Uterine sounds and acoustic stimulation of organoids

Source	Observed during	Frequency	Equivalent 100-Hz band SPL (dB re 20 µPa)	1-Hz spectrum level (dB re 20 µPa²/Hz)	PSD (Pa²/Hz)
(Vince et al., 1982)	Gestation	100 Hz	99	79	0.029
(Querleu et al., 1988)	Gestation	223…281 Hz	92	72	0.007
(Gerhardt et al., 1990)	Gestation	0...200 Hz	110-220	90-100	0.4-4
This study	Organoid maturation with heartbeat sound	100 Hz	98	78	0.027
This study	Short stimulation with heartbeat sound during Ca^{2+} imaging	100 Hz	125	105	13.180
This study	Short sound burst stimulation during Ca^{2+} imaging	150 Hz	122	102	5.800

Calcium imaging

For calcium imaging in HEK293-P1KO cell line, cells were plated on imaging dishes (#81156, Ibidi) and co-transfected with 500 ng of pGP-CMV-GCaMP6f (#40755, Addgene, Watertown, USA) and CMV>mPiezo1:IRES:mScarlet3 (#VB241021-1228apt, Vector Builder Inc, Chicago, USA) or empty plasmid pcDNA3.1 (#138209, Addgene) as control. Transient transfections were performed with lipofectamine 3000 transfection reagent (#L3000015, Thermo Fisher Scientific, Oberhausen, Germany) following the manufacturer's instructions.

For calcium imaging in human iAstrocytes, the cells were plated on Matrigel coated
imaging dishes and the pAAV[Exp]-GFAP(short)>jGCaMP8s:IRES:mScarlet3:WPRE virus was
added at a multiplicity of infection (MOI) of $5*10^4$ for 3 hours. Calcium imaging was performed 1
week after transduction.

For calcium imaging in NPCs, the cells were plated on Matrigel coated imaging dishes
and cultivated until monolayer. Thirty minutes before the scans, the culture medium was replaced
with Neurobasal medium supplemented with 2% SM1 neuronal supplement and Fluo-4 AM at a
final concentration of 5 µM for 30 minutes. Calcium responses were recorded for 5-6 minutes per
region of interest including 1 minute baseline at 37°C using the Leica TCS SP8 confocal
microscope with a 20x objective. Single plane 129.42x129.42 µm images (pixel size 253x253 nm)
were acquired at 0.188 seconds per frame rate). Calcium spikes were detected as $(F_{max}-F_{min})/F_{min}$, using standard imageJ selection and measurement tools and custom-written Matlab
scripts (**Supplementary Code 1**).

Superresolution 3D STED (SuSHi) and 2P shadow imaging

For visualizing the extracellular environment in living organoids, we adapted the SuSHi
technique from (Tonnesen et al., 2018). For stability, the organoids were attached to glass-bottom
imaging dishes coated with 1:30 diluted Matrigel for 5-10 hours prior to imaging experiment.

3D STED microscopy was performed from the bottom of the organoid, starting 5 µm above
the attachment site to avoid potential artifacts from Matrigel coating. For 3D STED microscopy,
organoid culture medium was supplemented with 200 µM calcein. 3D STED microscopy was
performed using a Leica 3D gSTED SP8 microscope (93x glycerol immersion objective with motor
correction, HC PL APO 93x/1,30 GLYC motCORR STED WHITE, and 75% 3D STED). Motor
correction was adjusted for maximum resolution at 10 µm imaging depth. Z-stacks (125x125x15
µm, voxel size 61x61x150 nm) were obtained between 5 and 20 µm from the coverslip. Apparent
resolution was estimated by measuring the full width at half-maximum (FWHM) of the smallest
visible structures (**Supplementary Table 2**).

2P microscopy was performed from the top of the organoid, and resolution at 100 µm
depth was estimated by FWHM of the smallest detectable structures (**Supplementary Table 2**).
2P microscopy was performed using a Leica TCS SP8 (25x HCX IRAPO L 25x water immersion
objective, NA 0.95) microscope. ROIs (295.3x295.3x115 µm, voxel size 85x85x699 nm) were
scanned as z-stacks. The excitation laser (Titanium:Sapphire Chameleon Vision II) was tuned to
890 nm, and the 15% of 1.7 W output power was used. Emitted fluorescence (500 - 570 nm
detection wavelength) was collected using a hybrid detector.

Immunolabeling procedures

For immunocytochemistry, samples were fixed with 4% PFA for 10 min (2D cell cultures) or 30 min (organoids) at room temperature (RT). Permeabilization and pre-blocking was applied for 2 hours at RT (2D cells) and 5 hours (organoids) with PBS pH 7.0 containing 0.15% Triton X-100 (2D cells) or 0.3% Triton X-100 (organoids), 10% Chemiblocker and 2% donkey serum. Primary antibodies were applied overnight at 4˚C , and secondary antibodies conjugated to fluorescent dyes were used for detection. Nuclei were counterstained with DAPI.

To enable 3D confocal imaging of large organoid volumes, optical index of tissues was matched to the target objective immersion by sequential incubation in 50% and 97% 2,2′-thiodiethanol (TDE) for 20 minutes, followed by mounting in 97% TDE on imaging dishes.

Microscopy and immunofluorescence quantifications

Image stacks for marker protein quantification in organoids were acquired using the Leica 3D gSTED SP8 microscope with a 20x Plan-Apochromat objective, numerical aperture (NA) 0.8. ROIs (472.3x472.3x5.5 µm, 124x124x500 nm) were scanned as Z-stacks and converted to maximum intensity projections. Image analysis was performed using standard tools in ImageJ.

High-resolution images for synapse quantification in organoids were acquired using the confocal microscope LSM710 (Carl Zeiss) with a 63x Plan-Apochromat objective (NA 1.4). Three random ROIs (90x90x5.5 µm, voxel size 88x88x457 nm) per organoid were scanned Z-stacks. 3D synapse quantification was performed using the Synapse counter plugin for ImageJ (Dzyubenko et al., 2016)

High-density multielectrode (HD-MEA) electrophysiology

Spontaneous activity was recorded using the BioCAM DupleX paired with CorePlate 1W 38/60 MEA plates (3Brain AG). Organoids were plated onto the electrode field, and immobilized for recording with the 3D printed meshes (3Brain GmbH, Lanquart, Switzerland). Before recordings, organoids were equilibrated for 1 hour in the incubator. Network activity was recorded for 5 minutes at 37°C using Brainwave 5 software. The recordings were acquired at 20 kHz sampling rate.

Biomimetic ECM hydrogels

Biomimetic hydrogels with adjustable stiffness were produced using the HyStem-HP Hydrogel Kit (Advanced Biomatrix) according to manufacturer's instructions. Gel stiffness was tuned to 0, 57, and 120 Pa shear storage moduli by adjusting the concentration of crosslinking reagent (PEGDA). Before polymerization, gel components were pre-mixed with the cultivation

medium and applied in 250 μl droplets onto astrocytic monolayers. After 2 hours, the gels were
completely polymerized, and Ca^{2+} imaging was performed 24 hours later.

LC-MS-MS proteomics

Human cortical organoids or mouse primary astrocytes were washed in cold PBS and
lysed in 30 μl of lysis buffer (Tris-HCl, 150 mM NaCl, 1% SDS, pH 7.8) supplemented with
complete mini EDTA free protease inhibitor. Samples were treated with 2,5 U Benzonase and
sonicated in a water bath twice for 5 minutes each, and centrifuged at 5000 g for 10 min to remove
cell debris. Protein concentration was determined using a BCA assay.

Tryptic digestion was performed for 16 hours at 37° C using the single-pot, solid-phase-
enhanced sample preparation (SP3) protocol (Hughes et al., 2019) with trypsin-to-protein ratio of
1:30. Eluted peptides were dried in an Eppendorf Concentrator Plus (Eppendorf SE, Hamburg,
Germany) and stored at minus 80° C until further use. Directly prior to measurement, peptides
were reconstituted in 20 μl of 0.1% FA and centrifuged at 16,000 g for 5 minutes to remove
remaining beads. The peptide concentration was estimated using a NanoDrop Microvolume
Spectrometer (Thermo Fischer Scientific, Waltham, USA) at 205nm.

For human cortical organoids, 50 ng of peptides were loaded onto an Evotip (Evosep
Biosystems, Odense, Denmark) following the manufacturer instructions. Peptide separation was
performed on an Evosep One (Evosep Biosystems, Odense, Denmark) using the predefined
Wisper Zoom 40 SPD method on an Aurora Elite CSI size C18 UHPLC column (15 cm length, 75
um inner diameter, 1.7 μm particle size, 120 Å pore size (IonOpticks, Collingwood, Australia)).

For primary mouse astrocytes, 200 ng of peptides were injected into a Nanoelute2 LC
system (Bruker Daltronics, Brillerica, Massachusetts, USA). Peptides were loaded onto a PepMap
Neo Trap Cartridge (5 mm length, 300 um inner diameter, 5 um particle size, 100 Å pore size;
Thermo Fisher Scientific, Massachusetts, USA) and analyzed using a 50-min chromatography
gradient on an Aurora Ultimate CSI 18 capillary column (25 cm length, 75 um inner diameter, 1.7
um particle size, 120 Å pore size (IonOpticks, Collingwood, Australia) consisting of mobile phase,
A (0.1% FA in H20) and mobile phase B (0.1% FA in ACN-H2O), ranging from 2-34% B at a flow
rate of 300nL/min.

Eluting peptides were injected into an TimsTOF HT mass spectrometer (Bruker Daltronics,
Brillerica, Massachusetts, USA), via a CaptiveSpray source at 1600V. The mass spectrometer
was operated in data-independent acquisition (DIA) PASEF mode. The accumulation and ramp
time for the dual TIMS analyzer were set to 100ms at a ramp rate of 9,42 Hz. Scan ranges were
set to m/z 100-1700 for the mass range and 1/k0 0.60-1.60Vs-1cm-2 for the mobility range at both
MS levels. For DIA-PASEF, a cycle time of 1.8 seconds was estimated. Within each cycle, a

precursor mass range of 400 to 1201 Da and a mobility range of 0.6 to 1.6 1/K0 was fragmented.

At MS1 level, one ramp was executed per cycle. For MS/MS measurements 32 MS/MS windows

with a mass width of 26.0 Da each and a mass overlap of 1.0 were distributed across the 16

MS/MS ramps.

Single-cell RNA sequencing

Single-cell suspensions were obtained by digesting 20 organoids per condition in 1 ml of

lysis buffer containing 30U of papain, 13mM of L-cysteine, and 125 U of DNase1. The lysis buffer

was pre-activated for 20 minutes at 37°C, and the organoids were dissociated using a rotary

shaker at 500 rpm and 37°C for 45 min and by pipetting up and down every 5 minutes.

In each sample, between 12.000 and 20.000 cells were loaded onto a GEM-X single-cell

3' chip. Sequencing-library construction was performed by following the GEM-X 3' assay v4 (10x

Genomics) protocol. Sequencing was performed using the Novaseq (Illumina) platform aiming for

30k reads per cell.

QUANTIFICATION AND STATISTICAL ANALYSIS

ECS volume

Segmentation of cellular and extracellular organoid compartments for ECS volume quantifications

in 3D STED and 2P shadow imaging was performed using trainable Weka segmentation in

ImageJ. Raw images were preprocessed, non-organoid masks detected by custom plugin and

subtracted from the segmented extracellular space (**Fig. S2** and **Supplementary Code 2**).

Spontaneous activity

For spike detection, the high-pass filter (100 Hz) was applied, and the sliding window

differential threshold algorithm implemented in Brainwave 5 software. A threshold of 9*SD of the

noise was used, sliding window length 2ms, and the timestamps were assigned to the negative

peak of the action potentials. For spike sorting we used the Legendre moments algorithm for

feature extraction paired with a K-means & Silhouette algorithm for clustering. Mean firing

frequency of each active unit was calculated for the entire recording time. Only units with a mean

firing frequency higher than 0.05 Hz were considered. Bursts were defined as series of 5

consecutive spikes occurring within a 100ms window.

LC-MS-MS data quantifications

LC-MS raw data were processed using the direct DIA algorithm in Spectronaut (Version
19.1.240806.626, Biognosys, Schlieren, Switzerland), applying BSG factory settings (Enzyme/
Cleavage rules: Trypsin/P; Fixed modification: Carbamidomethyl (C); Variable modifications:
Acetyl (Protein N-term) and Oxidation(M)), against a reviewed human UniProt/Swissprot FASTA
database (from 13th of March 2024, containing 20418 target sequences) for human cortical
organoids and against a reviewed murine UniProt/Swissprot FASTA database (from 13th of
March 2024, containing 17196 target sequences). Quantification was performed at the MS2 level.
Imputation was disabled. Cross run normalization was enabled. Normalized protein abundance
was used for further downstream analysis, exported and analyzed in R.

Protein abundances were log2 transformed to approach the Gaussian probability
distribution. Differentially abundant proteins between multiple predefined phenotypes were
determined by analysis of variation (ANOVA). Significantly regulated proteins (p<0.05) were
subjected to further analysis. Differentially abundant proteins between pairs of predefined
phenotypes were determined by Student's t-testing. Proteins showing significant differences
(p<0.05, fold change > 1.5) were subjected to further analysis. Heatmaps were generated based
on hierarchical clustering results. The Pearson correlation was used as a distance metric at the
sample and protein level respectively. Ward.D2 linkage was applied. Prior to heatmap generation,
log2 protein abundances were centered around the mean per protein for visual purposes. For
principal component analysis, a missing data-tolerant nonlinear PCA (NIPALs-PCA) was used.

Single-cell RNA sequencing quantifications

Raw sequencing data was processed using CellRanger (version 9.0.1) and aligned to the
human reference genome (GRCh38). Initial quality control was performed to retain cells with more
than 1000 and less than 8000 detected genes, and less than 10% mitochondrial reads. Doublets
were identified and removed using DoubletFinder (rate=8%). After quality filtering, a total of
44,743 cells remained for downstream analysis.

Data integration and clustering were performed using the Seurat package (Hao et al.,
2024) in R. The filtered data was processed using NormalizeData, FindVariableFeatures, and
ScaleData functions. Dimensionality reduction was first performed using RunPCA. Batch effects
between different experimental conditions were then corrected using Harmony (Korsunsky et al.,
2019) integration based on the PCA results. Visualization was achieved using RunUMAP, and
unsupervised clustering was performed using FindNeighbors and FindClusters based on the
Harmony embeddings with dims = 1:20 and resolution = 0.3. Cortical organoid single-cell spaces

were manually cured by removing fibroblasts. All violin plots, heatmaps, and feature plots were

drawn using standard plotting functions from R, Seurat, and SeuratExtend package (Hua et al.,

2025). Astrocyte signature intensities were measured using the Bioconductor package AUCell

(Aibar et al., 2017).

Statistical analysis of imaging and electrophysiology data

Data were analyzed in OriginPro2025 (OriginLab, Northampton, MA, U.S.A.). The

normality of data distributions was verified by Shapiro-Wilk mothod. Differences between group

means were analyzed using one or two -way mixed model ANOVA with Tukey's multiple

comparisons adjustment, followed by pairwise posthoc comparisons using t-tests. In all

experiments, the significance level was set as α=0.05, and the $p<0.05$ values indicated significant

differences between groups.

Table 2. Key resources.

REAGENT or RESOURCE	SOURCE	IDENTIFIER
Antibodies		
Sheep polyclonal anti-Neurocan	R&D Systems	Cat# AF6508
Mouse monoclonal anti-GLUA1 (extracellular)	Synaptic Systems	Cat# 182 011
Rabbit polyclonal anti-Vglut1	Synaptic Systems	Cat# 135 303
Guinea Pig polyclonal anti-MAP2	Synaptic Systems	Cat# 188 004
Rat monoclonal anti-GFAP (clone 2.2B10)	ThermoFisher	Cat# 13-0300
Rabbit polyclonal anti-SOX2	Abcam	Cat# ab97959
Mouse monoclonal anti-Nestin (clone 110C2)	StemCell Technologies	Cat# 60091AD
Mouse monoclonal anti-OCT4 (clone 3A2A20)	StemCell Technologies	Cat# 60093AD
STARRED FluoTag-X4 anti-Rabbit IgG	NanoTag	Cat# N2404
Alexa647 anti-Sheep IgG (H+L)	Jackson Immuno	Cat# 713-605-003
Alexa488 anti-Mouse IgG (H+L)	Life Technologies	Cat# A21202
Alexa594 anti-Rat IgG (H+L)	Life Technologies	Cat# A21209
Alexa647 anti-Genea Pig IgG (H+L)	Jackson Immuno	Cat# 706-605-148
Bacterial and virus strains		
pAAV[Exp]-GFAP(short)> jGCaMP8s:IRES:mScarlet3:WPRE	VectorBuilder	#AAVdjM(VB241018-1367mxv)-K1
Chemicals, peptides, and recombinant proteins		
hESC-grade Matrigel	Corning	Cat# 354277
mTeSR Plus medium	StemCell Technologies	Cat# 100-0276
STEMdiff SMADi neural induction medium	StemCell Technologies	Cat# 08581
Y-27632	StemCell Technologies	Cat# 72302
STEMdiff Neural Rosette Selection Reagent	StemCell Technologies	Cat# 05832
STEMdiff Neural Progenitor Medium	StemCell Technologies	Cat# 05833
STEMdif Astrocyte Differentiation Kit	StemCell Technologies	Cat# 100-0013
STEMdiff Astrocyte Serum-Free Maturation Kit	StemCell Technologies	Cat# 100-1666
STEMdif Dorsal Forebrain Organoid Differentiation Kit	StemCell Technologies	Cat# 08620
STEMdiff Neural Organoid Maintenance Kit	StemCell Technologies	Cat# 100-0120
Accutase	StemCell Technologies	Cat# 07920
cytosine-1-β-D-arabinofuranoside (AraC)	Sigma-Aldrich	Cat# C6645
DMEM	Gibco	Cat# 11966
B27	Gibco	Cat# 17504-001
poly-D-lysine	Sigma-Aldrich	Cat# A-003-E
TAT-Cre recombinase	Sigma-Aldrich	Cat# SCR508
Papain	Sigma-Aldrich	Cat# P3125
L-cysteine	Sigma-Aldrich	Cat# 5501

DNase 1	Roche	Cat# 11284932001
Protease inhibitors	Roche	Cat# 11836170001
Lipofectamine 3000	ThermoFisher	Cat# L3000015
Neurobasal medium	Life Technologies	Cat# A2477501
SM1 supplement	StemCell Technologies	Cat# 05711
Fluo-4	ThermoFisher	Cat# F14201
Calcein	Biotium	Cat# 80013
Lycifer Yellow	Sigma-Aldrich	Cat# L0259
DAPI	Sigma-Aldrich	Cat# D9542
Chemiblocker	Millipore	Cat# 2170
2,2'-thiodiethanol	Sigma-Aldrich	Cat# 166782
HyStem-HP Hydrogel Kit	Advanced Biomatrix	Cat# GS315F
Fetal bovine serum	Gibco	Cat# A5256701
Penicillin-streptomycin	Gibco	Cat# 15070-063
L-glutamine	PAN Biotech	Cat# P04-80050
Triton X-100	Calbiochem	Cat# 648462
Donkey serum	Sigma-Aldrich	Cat# D9663
Sodium chloride	Carl Roth	Cat# 9265.2
ROTI Stock 20 % SDS	Carl Roth,	Cat# 1057.1
Complete mini-EDTA free tablets	Roche	Cat# 11836170001
Benzonase Nuclease	Sigma-Aldrich	Cat# E1014-5KU
1.4- Dithiothreitol (DTT)	Roche	Cat# 10708984001
Iodoacetamide (IAA)	Sigma Aldrich	Cat# I1149-5G
Tris ultrapure	Applichem	Cat# A1086
Ammonium Bicarbonate (ABC)	Sigma Aldrich	Cat# 09830-500G
Calcium chloride solution, CaCl2	Sigma Aldrich	Cat# 21115-250ML
Sequencing grade Modified Trypsin	Promega	Cat# V5111
Dimethyl sulfoxide (DMSO)	Sigma Aldrich	Cat# D5879-100ML
Formic Acid 99+%	Thermo Scientific	Cat# 289905
Acetonitril (ACN), LC-MS Grade	Thermo Scientific	Cat# 51101
2-Propanol ROTISOLV ≥99,95 %, LC-MS Grade	Carl Roth	Cat# AE73.2
Water for LC-MS	Applichem	Cat# 701074.1611
Evotip Pure, Tips	Evosep	Cat# EV2013
Ethanol ROTISOLV ≥99,95 %, LC-MS Grade	Carl Roth	Cat# 1HP8.1
Sera-Mag Magnetic Carboxylate	Cytiva	Cat# 44152105050250
Sera-Mag Magnetic Carboxylate	Cytiva	Cat# 24152105050250
Critical commercial assays		
BCA assay	ThermoFisher	Cat# 23225
Deposited data		
Raw and analyzed proteomic data	This paper, PRIDE database	PRIDE token
Raw and analyzed transcriptomic data	database	GEO token
Raw and analyzed	Dryad database	Dryad token

Experimental models: Cell lines		
Healthy Control Human iPSC Line, Female, SCTi003-A	StemCell Technologies	Cat# 200-0511
Human iPSC-Derived Neural Progenitor Cells	StemCell Technologies	Cat# 200-0620
HEK293-P1KO	Ardem Patapoutian's lab	(Dubin et al., 2017)
Experimental models: Organisms/strains		
Rosa-CAG-LSL-GCaMP6f (Ai95D) mice	The Jackson Laboratory	Strain #028865
Oligonucleotides		
Recombinant DNA		
CMV>mPiezo1:IRES:mScarlet3	VectorBuilder	#VB241021-1228apt
pGP-CMV-GCaMP6f	Addgene	#40755
pcDNA3.1	Addgene	#138209
Software and algorithms		
R software environment version 4.1.2	The Comprehensive R Archive Network (CRAN)	https://ftp.fau.de/cran/
Seurat package (version 5.3.0)	(Hao et al., 2024)	https://cran.r-project.org/web/packages/Seurat/index.html
SeuratExtend (version1.2.3)	(Hua et al., 2025)	https://github.com/huayc09/SeuratExtend
Harmony (version 1.2.3)	(Korsunsky et al., 2019)	https://cran.r-project.org/web/packages/harmony/index.html
Bioconductor package AUCell	(Aibar et al., 2017)	https://bioconductor.org/packages/release/bioc/html/AUCell.html
OriginPro 2025 version (64-bit) SR1	OriginLab Corporation	https://www.originlab.com/
ImageJ	(Schneider et al., 2012)	https://imagej.nih.gov/ij/
Other		
AggreWell 800 24-well plates	Stem Cell Technologies	Cat# 34850
Glass Bottom Dish 35 mm	Ibidi	Cat# 81218-200
Hydrophone	Hottinger Brüel & Kjær	Cat# 8103

AK-45 Digital Audio Amplifier	sikkeby	https://www.amazon.de/HiFi-Verst%C3%A4rker-Stereo-Audioverst%C3%A4rker-Endverst%C3%A4rker-Soundverst%C3%A4rker-USB-Karteneingang/dp/B0BXD288TM?th=1
Flatpanel CT-17803 loudspeaker	ChiliTec	https://www.amazon.de/products_id-78311-Flatpanel-Lautsprecher-40W-schwarz/dp/B00BVZX1KE/ref=ast_sto_dp_puis
MP3 Sound-Chip Module	WayinTop	https://www.amazon.de/WayinTop-Beschreibbares-Programmierbare-Herunterladbar-Aufladbarer/dp/B07X7G7DZG/ref=ast_sto_dp_puis
Supplementary audio file 1	This paper	n/a
Supplementary audio file 2	This paper	n/a
Supplementary Video 1	This paper	n/a
Supplementary Video 2	This paper	n/a
Supplementary Video 3	This paper	n/a
Supplementary Video 4	This paper	n/a
Supplementary Video 5	This paper	n/a
Supplementary Video 6	This paper	n/a
Supplementary Video 7	This paper	n/a
Supplementary Video 8	This paper	n/a

SUPPLEMENTARY FILES AND CODE

Supplementary Videos 1-8

Supplementary Codes 1-3

Supplementary audio files 1-2

Supplementary figures and tables

Supplementary Table 1. Shadow imaging resolution.

	3D STED	2P
	10 µm depth	100 µm depth
n	FWHM, nm	FWHM, nm
1	150	540
2	130	460
3	210	320
4	130	400
5	140	590
6	150	440
7	120	310
8	130	
9	150	
10	120	
11	200	
12	180	
13	210	

596 **Supplementary Table 2. Astrocyte clusters and their function.**

	Cluster name	Upregulated genes	Rationale
		Astrocyte-enriched organoids	
0	Neurotrophic & Synaptogenic	MDK, IGFBP2, RSPO3, FBLN1, CDH7, TSPAN7, NELL1, ITM2C/BRI2, CLYBL, SPARCL1, WNT7B	Astrocytes enriched for trophic and axon-guidance factors (MDK, IGFBP2, NELL1), Wnt potentiation (RSPO3), ECM assembly (FBLN1), adhesion (CDH7) and EV-linked synapse modulators (TSPAN7), consistent with astrocyte-driven synapse maturation and astro support. These cells likely enhance neurite growth and synaptogenesis while stabilizing the perisynaptic microenvironment.
1	Perisynaptic & Homeostatic	GJA1, DBI, SCD, TXNIP, MT2A, CPE, PMP2, S100B, EDNRB, AHCYL1, ID2, GABBR2, PCDH9, BCAN	Defined by canonical astrocyte markers (S100B, GJA1, DBI, MT2A, TXNIP) plus BCAN, PCDH9, and GABBR2, this state is related to synapse regulation and homeostatic astrocyte responses to Ca^{2+} oscillations
2	Perisynaptic & Dynamic	DBI, TXNIP, BCAN, AHCYL1, TFPI, WLS, CREB1L, ARID5B, FSTL5, SNCAIP, EDNRB, ID2	Characterized by Wnt secretion (WLS), synapse interaction adhesion molecules (FSTL5, SNCAIP), and CREB-mediated transcriptional reprogramming, this state combines homeostatic ECM support (BCAN, DBI, TFPI) with enhanced potential for synaptic remodeling and plasticity
3	Synapse adhesion	PCDH9, ADGRB3, TNIK, GREB1L, PPP2R2B, LRRC4C, MIR99AHG, GLIS3, CTNND2, SNCAIP, FSTL5, NEAT1	Enrichment of synapse adhesion regulators together with NEAT1, defines a perisynaptic, adhesion-rich astrocyte state that stabilizes and modulates synaptic contacts; reduced ribosomal/EIF1/RACK1 and vimentin indicates a mature, low-biosynthesis, non-reactive profile
4	Biosynthetic	PMP2, MT2A, SCD, DBI, S100B, RACK1, FTH1, RPLP1, RPLP0, RPL15, RPS28, RPL13A, RPL13 RPS14, RPS8, RPL41	Marked by ribosomal gene enrichment and reduced developmental adhesion programs (NFIA, ZBTB20, NPAS3, RORA; LSAMP, ADGRV1), this state reflects a translation-high phenotype

5	Vesicle-trafficking & Synaptogenic	CD9, CDH7, S100A10, S100A6, TSPAN7, NELL2, CAV1, ETNPPL, ANXA2, YBX3, VIM, SPARCL1	Enrichment of tetraspanins and vesicle-associated genes defines an astrocytic phenotype specialized for exosome- and caveolae-mediated membrane trafficking and intercellular signalling
6	Stressed & Activated	RACK1, UCHL1, SQSTM1, CEBPB, CCPG1, SARS, DDIT3, TCEA1, HSPA9, EIF1	This phenotype combines adaptive responses to stress with reduced protein synthesis and upregulated hypoxia-activated genes
7	Neural patterning & guidance	ZBTB20, EIF4G3, LSAMP, PHACTR1, NFIA, ADGRV1, NPAS3, LRP1B, RORA, NELL1, GLIS3, KALRN	Enrichment of transcriptional factors associated with differentiation, morphogenesis, and adhesion indicates a patterning and contact-guidance astrocytic phenotype
8	Angiogenic & motile	PTN, NR2F2-AS1, PDE1A, EEF1A1, H3F3A, WNT7B, NR2F2, C1orf61, FABP7, RND3, MARCKSL1	This cluster combines neurovascular signature (WNT7B, NR2F2, PTN) with a radial glia like expression (FABP7, RND3, MARCKSL1) and Ca^{2+} signaling, indicating these astrocytes can migrate and promote vascular development.
9	Perivascular & homeostatic	S100A6, KCTD1, LHFPL6, NKX2-1, MGP, ATP1A2, EMP2, CALD1, CYSTM1, APOE	This phenotype shows genes related to astrocytic end feet at blood-brain barrier interfaces (ATP1A2, APOE, EMP2, CALD1), secreted matricellular cues (SPARCL1, CD9, S100A10, ANXA2), and ventral telencephalon identity (NKX2-1)
10	Neuronal signature	GRIA2, DLGAP1, NRXN1, ANK3, MYT1L, KALRN, NAV3	Canonical neuronal gene expression associated with neurite and synapse development, possibly indicating phagocytic astrocytes contributing to synaptophagy and therefore incorporating neuronal mRNA

		Cortical organoids without astrocyte enrichment	
0	Neurotrophic & Synaptogenic	ETNPPL, PLP1, RSPO3, WNT7B, PHACTR1, RMST, NR2F2-AS1, SPARCL1, ADGRV1, ADAMTSL1, FBLN1, NRXN3, CSRP2, NELL2, AC092957.1	Astrocytes strongly expressing neurotrophic and synaptogenesis regulators (RSPO3/WNT7B) together with synapse-promoting (SPACRL1) and ECM/adhesion organizers (NRXN3, ADGRV1, ADAMTSL1, FBLN1), consistent with astrocytes that produce trophic cues and actively promote excitatory synaptogenesis.
1	Homeostatic & Secretory	PTGDS, MT3, C1orf61, CPE, B2M, ID2, CLU, PI15, PCDH9, PPP2R2B	Homeostatic astrocytes enriched with secreted chaperones and neuroprotective signals (CLU, CPE, PTGDS, MT3), while expressing synapse-associated molecules (PCDH9/PPP2R2B) to stabilize and tune astrocyte-neuronal interactions
2	Synaptogenic & ECM-remodeling	CST3, SPARCL1, S100A10, ADAMTSL1, CD9, TNC, LGALS1, FBLN1, CSRP2, NELL2	These astrocytes promote and stabilize excitatory synapses (SPARCL1, CSRP2) exporting extracellular vesicles (CD9), and sculpting perisynaptic matrix (CST3, ADAMTSL1, TNC, FBLN1/ADAMTSL1)
3	Stress-adaptive	FTL, FTH1, CDKN1A, EIF1, RACK1, TKT, RPS27L, RPL19, RPS13, GAS5	Astrocytes with upregulated DNA repair (CDKN1A, RPS27L), antioxidant response (GAS5, TKT, RACK1, EIF1) and ferroptosis-regulating genes (FTH1, FTL).
4	Hypoxia-adaptive	IGFBP2, IGFBP5, BNIP3, VEGFA, PGK1, TRIM2, SLC2A1, FAM162A, HILPDA, P4HA1	These astrocytes show the hypoxia-associated metabolic switch pattern (GLUT1, PGK1, VEGFA), cellular remodeling (BNIP3, HILPDA, P4HA1), and trophic control (IGFBP2/5) in hypoxic niches.
5	Neuronal signature	ANK3, NAV3, SNHG14, GRIA2, CELF4, FAM155A, FGF14, NLGN1, PPFIA2, DLG2	This cluster is enriched with canonical neuronal transcripts found in axons (ANK3, NAV3) and synapses (FGF14, GRIA2, DLG2, NLGN1, PPFIA2), possibly indicating synaptophagic astrocytes

Supplementary Figure 1. Generation of astrocyte-enriched human cortical organoids.

(**A**) Without astrocyte enrichment, cortical organoids at day 45 contained few astrocytes (GFAP, green).
(**B**) For astrocyte enrichment, pre-differentiated human induced astrocytes (iAstrocytes, GFAP, yellow)
were co-cultured with neural precursor cells (NPCs) during organoid formation. (**C**) Astrocyte-enriched
organoids develop networks of ramified astocytes (GFAP, green), mature neurons (MAP2, red), and
establish glutamatergic synapses (VGLUT1m cyan) at 45 days of cultivation. (**D**) Gene ontology cellular
component analysis (GOCC) based on significantly regulated proteins (p < 0.05, fold change difference >
1.5, t-test) measured with LC-MS/MS. The analysis shows upregulated extracellular matrix, secretory
programs, and synaptic proteins in astrocyte-enriched vs non-enriched organoids (n=6). Scale bars, 50 µm.
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Supplementary Figure 2. Shadow imaging and image processing.

(**A**) Strategy for visualizing the organoid extracellular space (ECS). Organoids were attached to glass-bottom imaging dishes coated with 1:30 diluted Matrigel for stability. 3D STED microscopy was performed from the bottom of the organoid, starting 5 µm above the attachment site to avoid potential artifacts from Matrigel coating. Apparent resolution at 10 µm depth was estimated by measuring the full width at half-maximum (FWHM) of the smallest visible structures. 2P microscopy was performed from the top of the organoid, and resolution at 100 µm depth was estimated by FWHM of the smallest detectable structures. (**B, C**) Segmentation of cellular (red) and extracellular (green) organoid compartments for ECS volume quantifications in 3D STED and 2P shadow imaging.

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Supplementary Figure 3. Shadow imaging and ECS volume in human cortical organoids without
astrocyte enrichment.
(**A**) Superresolution 3D STED shadow imaging and ECS segmentation (red) in live organoids. (**A'**) ECS
volume fraction comparison, t-test (n=10-15). (**B**) 2-photon shadow imaging and ECS segmentation (red)
in live organoids. (**B'**) ECS volume fraction comparison, t-test (n=5-6). (**C**, **D**) Images are xy and zy
projections; LUT inverted. Scale bars, 50 μm.

Supplementary Figure 4. ECM proteins regulated by heartbeat.

Heatmap shows normalized, centered log2 protein abundances for ECM proteins found significantly different (p<0.05, t-test) between astrocyte-enriched+control versus astrocyte-enriched+heartbeat groups.

632 **Supplementary Figure 5. Cellular composition of cortical organoids without astrocyte enrichment.**

633 (**A**) Transcriptomic UMAP map generated from scRNAseq data shows key cellular lineages. (**B**) Astrocyte

634 subtypes revealed by cluster analysis of astrocytic transcriptomes (see **Fig. S6** and **Supplementary**

635 **Table 2** for functional interpretation).

Supplementary Figure 6. Astrocytic subpopulations identified by scRNA sequencing.

Heatmaps show z-scores of key genes differentially expressed in astrocytic subpopulations identified by unsupervised cluster analysis. For functional interpretation, see **Supplementary Table 2**.

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Supplementary Figure 7. Synapse-associated proteins regulated by heartbeat.
Heatmap shows normalized, centered log2 protein abundances for synapse-regulating proteins found
significantly different (p<0.05, t-test) between astrocyte-enriched + control versus astrocyte-enriched +
heartbeat groups.

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Supplementary Figure 8. Synaptogenesis in astrocyte-enriched and non-enriched organoids.
(**A**) Immunolabeling of neurons (MAP2, magenta), astrocytes (GFAP, yellow), and neurocan (NCAN, cyan)
indicates the enrichment of ramified astrocytes, quantified in (**C**) as the GFAP/MAP2 fluorescence intensity
ratio (n=7). (**B**) Immunohistochemical analysis of synaptic markers VGLUT1 (magenta) and AMPA receptor
subunit GLUA1 (cyan). Neuronal dendrites are labeled with MAP2 (yellow). (**A, B**) Nuclei (blue) are
counterstained with DAPI. Scale bars, 50 µm. (**D**) Quantifications of GLUA1, VGLUT1 synaptic puncta, and
their overlaps. (n=9). (**C, D**) Intergroup differences were analyzed by two-way ANOVA followed by t-tests.
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Supplementary Figure 9. Direct acoustic stimulation in the medium. (A) Custom-made device for direct acoustic stimulation in the medium. A miniature loudspeaker (8 Ohm, 1 Watt) was attached to the lid of an Ibidi dish used for confocal imaging. To achieve the direct transfer of acoustic waves produced by the loudspeaker, a circular coupler was glued to the loudspeaker membrane. The recorded heartbeat was played via an MP3 player with a trigger. (B) Hydrophone recording and power spectrum of the applied heartbeat stimulation.

Supplementary Figure 10. Ca²⁺ responses to heartbeat sound stimulation in NPCs. Averaged Ca^{2+} responses evoked by heartbeat and 10 µM Yoda1 application in NPCs were measured using the Fluo-4 Ca^{2+} indicator. (14-20 cells, n=5)

Supplementary Figure 11. Ca²⁺ responses to heartbeat sound stimulation in HEK293 cells. Averaged Ca^{2+} responses evoked by co-application of 0.01 µM Yoda1 and heartbeat sound stimulation (47 cells, n=7)

Supplementary Figure 12. Ca²⁺ responses to low-frequency sound stimulation in primary mouse astrocytes.

(**A**) Hydrophone recording and power spectrum of short 150 Hz frequency sound burst stimulation. (**B**) Averaged Ca²⁺ responses to short (1 s) sound bursts in HEK293-P1KO cells co-transfected with PIEZO1-mScarlet (orange) or Mock control (blue) and GCaMP6f. Co-application of a non-activating 0.01 μM Yoda1 concentration and sound bursts amplified PIEZO-mediated Ca²⁺ responses (49-62 cells, n=7). (**C**) Primary astrocyte cultures were prepared from Ai95 (Rosa-CAG-LSL-GCaMP6f) mice, and GCaMP6f expression was induced by TAT-iCre recombinase. One week later, astrocytes were replated onto glass-bottom imaging dishes, and Ca²⁺ imaging was performed in monolayers 2 weeks after replating. Scale bars, 100 μm. (**D**) Ca²⁺ responses to three consecutive 1 s sound bursts delivered at 90-s intervals showed reduced amplitudes compared to the first response, indicating desensitization (21 cells, n=10). (**E**) Averaged Ca²⁺ responses to heartbeat stimulation in primary astrocytes (41 cells, n=12). (**D**) Comparison of different modes of PIEZO1 activation in astrocytes: a single 150-Hz sound burst with (62 cells, n=7) or without (43 cells, n=7) 0.01 μM Yoda1, heartbeat-like stimulation with (54 cells, n=8) or without (23 cells, n=4) 0.01 μM Yoda1, and 10 μM Yoda1 without acoustic stimulation (39 cells, n=5).

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Supplementary Figure 13. Protein expression changes induced by PIEZO1 activation in primary
mouse astrocytes.
(**A**) Heatmap shows normalized, centered log2 protein abundances for ECM proteins found significantly
different (p<0.05, t-test) between Yoda1 + sound burst stimulation versus Yoda1 stimulation versus control
astrocyte cultures, measured by LC-MS/MS. (**B**) Volcano plots show major regulations of intracellular
proteins induced in mouse astrocytes by Yoda1 + sound burst stimulation and Yoda1 stimulation versus
control, detected my LC-MS/MS.

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