Mapping long-term memory modulation with transcranial alternating current stimulation

Running title: Mapping long-term memory

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Abstract

Background: Long-term memory (LTM), which is the ability to retain information over a long period of time, is governed by neural oscillations in various parts of the cerebral cortex. To investigate the relationship between oscillations and memory performance, transcranial alternating current stimulation (tACS) has been used to modulate LTM. However, due to the variability in stimulation parameters and locations, no clear picture has arisen on where tACS needs to be applied to improve LTM.

Methods: We collected behavioral data from 20 studies (58 effect sizes) and computationally modeled the corresponding brain electric fields based on each study's unique tACS parameters. As a result, we generated a map of performance–electric field index (PEI) values using linear and quadratic fits.

Results: Theta-tACS showed no regions with a positive linear association with LTM. However, left lateral prefrontal and temporal areas exhibited negative associations, meaning that theta stimulation of that region led to decreased LTM performance. A quadratic analysis revealed an inverted-U relation in the right parietal cortex, suggesting improved memory at moderate, but not high, electric field strengths. Gamma-tACS showed positive linear associations in parieto-occipital cortex and negative ones in frontal regions. For gamma, we found no regions that expressed a quadratic relationship.

Conclusion: These findings indicate that LTM-relevant tACS effects are frequency- and site-specific and potentially nonlinear with respect to intensity. Integrating meta-analytic effect sizes with individualized field estimates provides a brain-wide framework for identifying targets of memory modulation and for guiding future fundamental and translational research.

Keywords: Transcranial Alternating Current Stimulation; Long-term Memory; Meta-analysis; Electric Field Modeling; Neural oscillations

Introduction

The ability to retain information from hours, days, weeks, or even months ago is one of the hallmarks of the brain[1]. Besides the importance of gaining a fundamental understanding of the underlying brain mechanisms, long-term memory (LTM) studies are critical for further expanding the treatment options for memory-related deficits, such as Alzheimer's disease or traumatic brain injury[2,3]. In rodent models, memory is most commonly studied in subcortical areas, including the hippocampus and the amygdala[4–6]. However, human studies tend to focus on various cortical regions involved in processing and retaining information, including prefrontal, parietal, and temporal structures [7–12]. Furthermore, within these regions, particular neural oscillations, such as theta (3-8 Hz) and gamma (30-200 Hz), have been highlighted through their association with encoding and retrieval of memory[13–15].

Previous studies have investigated the role of oscillations using neurophysiological recordings. Osipova et al[16] engaged their participants in a picture recognition task while magnetoencephalographic (MEG) data were recorded. They found higher theta and gamma power both during encoding when the picture was subsequently remembered (subsequent memory effect) and during retrieval, when distinguishing old pictures from new. Furthermore, intracranial recordings from epilepsy patients showed a similar pattern, with increases in theta and gamma power over several cortical regions for subsequent memory effects[17–19]. In contrast, Hanouneh et al[20] showed that theta power in prefrontal regions was negatively correlated with LTM retrieval. However, Scholz et al[21] showed that theta power is positively associated with memory encoding.

Given the correlational nature and variability in results of the studies using electrophysiological techniques, others have used neuromodulation methods to pinpoint regions that causally relate to memory performance[22–24]. One particular technique suited to study neural rhythms is transcranial alternating current stimulation (tACS) and various studies have used it to alter cortical oscillations during memory tasks[25–28]. By applying a sinusoidal low-intensity current to the scalp, tACS has been shown to entrain neural spiking, which can result in a modulation of endogenous oscillatory activity[29,30]. Besides these neurophysiological effects, various studies have shown that tACS is able to modulate human behavior and cognition[25,31,32]. The rationale is that the tACS-induced entrainment of neural oscillations is directly related to changes in behavioral performance. As an example, long-term face recognition was improved by applying theta tACS to the right posterior parietal region during encoding[33]. On the other hand, Manippa et al[26] found reduced LTM performance following gamma tACS over bilateral temporal areas.

In accordance with the breadth of results in MRI and EEG studies, tACS has been applied in LTM experiments at various cortical locations and frequencies. Given the variety in parameters and protocols, a classic meta-analytic approach is suboptimal to summarize the efficacy of tACS, nor to identify core functional regions of LTM. By integrating meta-analytic results with electric field modeling, this limitation can be overcome[34–37]. Using SimNIBS software tACS-induced electric fields can be estimated based on a particular stimulation location and intensity[38]. By correlating the electric field distributions of different studies with their corresponding behavioral effect sizes (on LTM in this case), a meta-analytic brain map is generated that displays where tACS leads to increased, decreased, or no change in task performance[35].

In the present study, we leverage the meta-modeling approach to summarize the effects of tACS on LTM. Thereby, we identify regions where neural oscillations in a given frequency are directly related to memory performance. Altogether, these results aim to complement previous research on cortical oscillations in LTM and point out cortical regions of interest for LTM research.

Methods

Sample

We collected effect sizes, expressed in Hedges' g from available literature. The data was obtained from articles published in peer-reviewed journals, pre-prints, and published theses, by searching through PubMed, Web of Science, ProQuest (Dissertations and Theses), BioRxiv and PsycINFO databases. The search was conducted in general accordance with the PRISMA guidelines[39]. First, articles were identified using the following search terms: ("tACS" OR "transcranial alternating current stimulation") AND ("memory"). After removal of duplicates, the texts underwent abstract and full-text screening. Inclusion of studies in our modeling is based on the following criteria: I) Articles are written in English, II) Full-text is available to the researchers, III) manuscripts allowed for extraction of effect size (based on mean and standard deviation) from text, tables, or figures, IV) the study used a control condition (e.g., placebo) to which active stimulation can be compared, V) the study was conducted on a healthy adult population (>= 18 years old), VI) tACS applied online or offline, but not during sleep, VII) long-term memory assessed explicitly. For the criteria, we rely on a broad definition of long-term memory as information retrieved from the past that does not rely on active maintenance[2]. A preliminary search suggested that 15-25 articles could be eligible, suggesting that enough data can be collected to perform our meta-modeling analyses. In total, the final search yielded 20 articles and 58 unique effect sizes (note that one study typically has multiple outcome measures). Across all studies n = 1210 healthy volunteers were included between the ages of 18-77. Since previously published data were used, no ethical approval was obtained.

Effect size calculation

The standardized effect sizes were expressed as Hedges' g values[40]. Hedges' g values express the ratio between differences in effects and the variability, similar to Cohen's d values[41], with the addition of a correction factor for small sample sizes. If Hedges' g values were reported, they were directly taken from the article. Alternatively, if the article provided the Cohen's d value, the correction factor was applied to calculate Hedges' g. If no effect size measures were directly reported, the Hedges' g was calculated based on reported averages and standard deviations or those estimated from graphs. All effect sizes used in this analysis reflect the difference between an active stimulation condition and a sham control. As such, positive g values reflect improved memory performance in active tACS conditions compared to sham, while negative g values relate to worsened memory performance in active tACS conditions compared to sham.

Electric field modeling

Electric field simulations were performed on 50 realistic head models (age range 22-35, 22 females). The head models were generated based on data from the Human Connectome Project S1200[42]. Quality and suitability for electric field modeling were assessed previously[43]. Each head model consists of 6 biological tissues, namely the skin, skull, cerebrospinal fluid, eyes, gray matter and white matter. For each tissue standard conductivity values were used ($\sigma_{skull} = 0.01$ S/m, $\sigma_{skin} = 0.465$ S/m, $\sigma_{CSF} = 1.654$ S/m, $\sigma_{graymatter} = 0.275$ S/m, and

σwhitematter = 0.126 S/m)[44,45]. Electrode location, orientation, and material were gathered from the articles and used for electric field modeling in SimNIBS 4.1[38]. For the purpose of this study, we extracted the induced electric fields from the gray matter, as this reflects the tissue at which tACS most likely induces functional changes[46,47]. In order to compare and average between head models, all electric field simulations were transformed into the normalized FreeSurver average (fsavg) standard brain. Importantly, by first performing simulations in the individual head models and then transforming them into fsavg space (rather than directly performing electric-field simulations in fsavg models), individual variability is still accounted for.

Calculation of the performance-electric field index

To relate different elements of fsavg model to functional brain regions, each element was categorized following the Human Connectome Project multimodal parcellation (HCP-MP) atlas[48,49]. This atlas parcellates the brain models into 360 function regions (180 per hemisphere). Given that we found 36 and 22 outcome measures for theta and gamma, respectively, and 360 functional regions, a 36 x 360 matrix and a 22 x 360 matrix of electric field values are obtained. This matrix is subsequently correlated with a vector of Hedges' g values for each row of the matrix (i.e., for each functional region), resulting in a 1 x 360 matrix that represents the correlation between electric fields and tACS-induced performance changes[34–37]. We refer to these values as the performance-electric field index (PEI). Besides this we report the uncorrected p-values. Note that due to the nature of meta-analytic datasets, no a priori power analysis was performed, and the number of data points depends on the available literature. As such, the exact p-value, and hence the optimal way to correct for multiple comparisons, is somewhat arbitrary. Therefore, we opted to report uncorrected p-values and visually represent them as $p<0.05$ (*), $p<0.01$ (**), and $p<0.001$ (***). For visualization, we categorized the 360 HCP-MP atlas region into 22 larger regions[50].

In addition to the linear correlation analysis, we performed an exploratory analysis testing for a potential quadratic relationship between electric field strength and performance. This analysis was performed as several studies have shown that the effects of tACS follow a U-shape[51–53] or inverted U-shape [54,55]. For each cortical region, we fit a linear ($y = \beta_0 + \beta_1 x$) and quadratic regression model ($y = \beta_0 + \beta_1 x + \beta_2 x^2$), with the behavioral effect size (Hedges' g) as the dependent variable and regional E-field magnitude as the predictor. For both linear and quadratic models, a correlation value was defined as the signed square root of R-squared, with the sign determined by the regression values being positive or negative. For each region, we determined the better-fitting model (linear or quadratic) based on adjusted R-squared. Across 50 head models, results were averaged per region. If more than 50% of the head models yielded a quadratic fit for a particular region, the quadratic correlation values were averaged. We refer to this value as the $PEI_{QUAD,}$ where positive and negative values correspond to a U-shaped and an inverted U-shaped relationship between electric field strength and performance, respectively.

Table 1. Overview of studies using theta tACS included in the meta-analysis.

Reference	Montage	Freq. (Hz)	Intensity (mA)	Task	Time between encoding and retrieval	Hedges' g
Alekseichuk et al., 2020	P4, T8/C2/CP1/Oz	4	3	face recognition	20 min	0.31
	P3, T7/C1/CP2/Oz	4	3	face recognition	20 min	0.06
Chantrel et al., 2021	F3, left wrist	6	1.5	word recognition	90 min	-0.32
	F3, left wrist	6	1.5	word recognition	7 days	-0.15
Ergo et al., 2020	FCz, neck	6	2	word association task	Immediate	-0.21
Grover et al., 2022	FP1/F1/FC3/F5/AF7/Afz, Fz/AF3/cheek	4	1.58	delayed recall, words	Immediate	0.01
	C3/T7/CP1/FC5/TP7FT7/PO7/cheek, CP5	4	1.58	delayed recall, words	Immediate	0.06
	C3/T7/CP1/FC5/TP7FT7/PO7/cheek, CP5	4	1.58	delayed recall, words	1 month	0.17
Klink et al., 2020	Intersection of T3/F3/C3/F7, rSOR	5	1	face-occupation task	20 min	-0.14
	Intersection of T3/F3/C3/F7, rSOR	5	1	face-occupation task	1 day	0.03
Komissarenko et al., 2025	F7, P7	5.5	1	word association recognition	1 min	-0.04
	F7, P7	5.5	1	word association recognition	4 days	-0.14
Lang et al., 2019	right fusiform 4x1	6	4	face-scene association	online	0.56
Meng et al., 2021	P3, ring surround	6	2	face-scene task, pictures	5 min	-0.42
Murray et al., 2023	T3, T4	6	1.5	delayed recall, words	20 sec	-0.47
Shtoots et al., 2024	Chin, P1/P2/P3/P4	3	1.5	delayed recall, pictures	2 hours	0.29
	Chin, P1/P2/P3/P4	3	1.5	delayed recall, pictures	1 day	0.39
	Chin, P1/P2/P3/P4	3	1.5	delayed recall, pictures	7 day	0.4
	Fz, AF4/AF3/FC2/FC1	3	1.5	delayed recall, pictures	2 hours	1.11
	Fz, AF4/AF3/FC2/FC1	3	1.5	delayed recall, pictures	1 day	1.27
	Fz, AF4/AF3/FC2/FC1	3	1.5	delayed recall, pictures	7 day	1.26
Shtoots et al., 2025	Chin, P1/P2/P3/P4	3	1.5	multiple choice exam, video	20 min	1.05
	Chin, P1/P2/P3/P4	3	1.5	multiple choice exam, video	1 day	0.73
	Chin, P1/P2/P3/P4	3	1.5	multiple choice exam, video	7 day	0.65
	P3, C3/TP7/Pz/O1	3	1.5	multiple choice exam, video	20 min	1.24
	P3, C3/TP7/Pz/O1	3	1.5	multiple choice exam, video	1 day	1.16
	P3, C3/TP7/Pz/O1	3	1.5	multiple choice exam, video	7 day	1.01
	Fz, AF4/AF3/FC2/FC1	3	1.5	multiple choice exam, video	20 min	0.67

	Fz, AF4/AF3/FC2/FC1	3	1.5	multiple choice exam, video	1 day	0.83
	Fz, AF4/AF3/FC2/FC1	3	1.5	multiple choice exam, video	7 day	0.91
Varastegan et al., 2022	FPz, Oz	6	2	delayed recall, words	20 min	1.06
Wynn et al., 2024	AF4/P5, Cz	4	2	word recognition	15 min	0.09
Wynn et al., 2020	P7/P8, Cz	3.5	2	word recognition	7 min	0.03
	P7/P8, Cz	3.5	2	screen location recognition	7 min	0.00
	P7/P8, Cz	8	2	word recognition	7 min	0.02
	P7/P8, Cz	8	2	screen location recognition	7 min	0.00

Table 2. Overview of studies using gamma tACS included in the meta-analysis.

Reference	Montage	Freq. (Hz)	Intensity (mA)	Task	Time between encoding and retrieval	Hedges' g
Ambrus et al., 2015	F3/F4, left/right mastoid	140	1	cued recall, words	10 min	-0.20
	F3/F4, left/right mastoid	140	1	cued recall, words	12 hours	0.00
Chantrel et al., 2021	F3, left wrist	60	1.5	word recognition	90 min	-0.21
	F3, left wrist	60	1.5	word recognition	7 days	-0.49
	C4, left wrist	60	1.5	word recognition	7 days	-0.12
Grover et al., 2022	FP1/F1/FC3/F5/AF7/Afz, Fz/AF3/cheek	60	1.58	delayed recall, words	Immediate	-0.01
	FP1/F1/FC3/F5/AF7/Afz, Fz/AF3/cheek	60	1.58	delayed recall, words	1 month	0.17
	C3/T7/CP1/FC5/TP7FT7/PO7/cheek, CP5	60	1.58	delayed recall, words	Immediate	-0.02
Javadi et al., 2017	F3, left wrist	60	1.5	word recognition	1.5 hours	0.38
	F3, left wrist	60	1.5	word recognition	1.5 hours	0.46
	F3, left wrist	60	1.5	word recognition	1.5 hours	0.02
	F3, left wrist	60	1.5	word recognition	1.5 hours	0.38
Luckey et al., 2022	Bilateral C2 dermatome	40	3	word association task	7 days	1.05
Manippa et al., 2024	T7, T8	40	2	delayed recall, words	4 min	0.08
	T7, T8	60	2	delayed recall, words	4 min	-0.13
Nomura et al., 2019	F3, left arm	60	1.5	word recognition	Immediate	0.21
	F3, left arm	60	1.5	word recognition	1 day	0.74
	F3, left arm	60	1.5	word recognition	6 days	1.17
Sun et al., 2025	P3, right deltoid	60	1.5	cued recall, words	4 min	0.35

	P3, right deltoid	60	1.5	cued recall, words	7 days	0.81
	P3, right deltoid	60	1.5	cued recall, words	28 days	1.09
Wynn et al., 2024	AF4/P5, Cz	50	2	word recognition	15 min	0.10

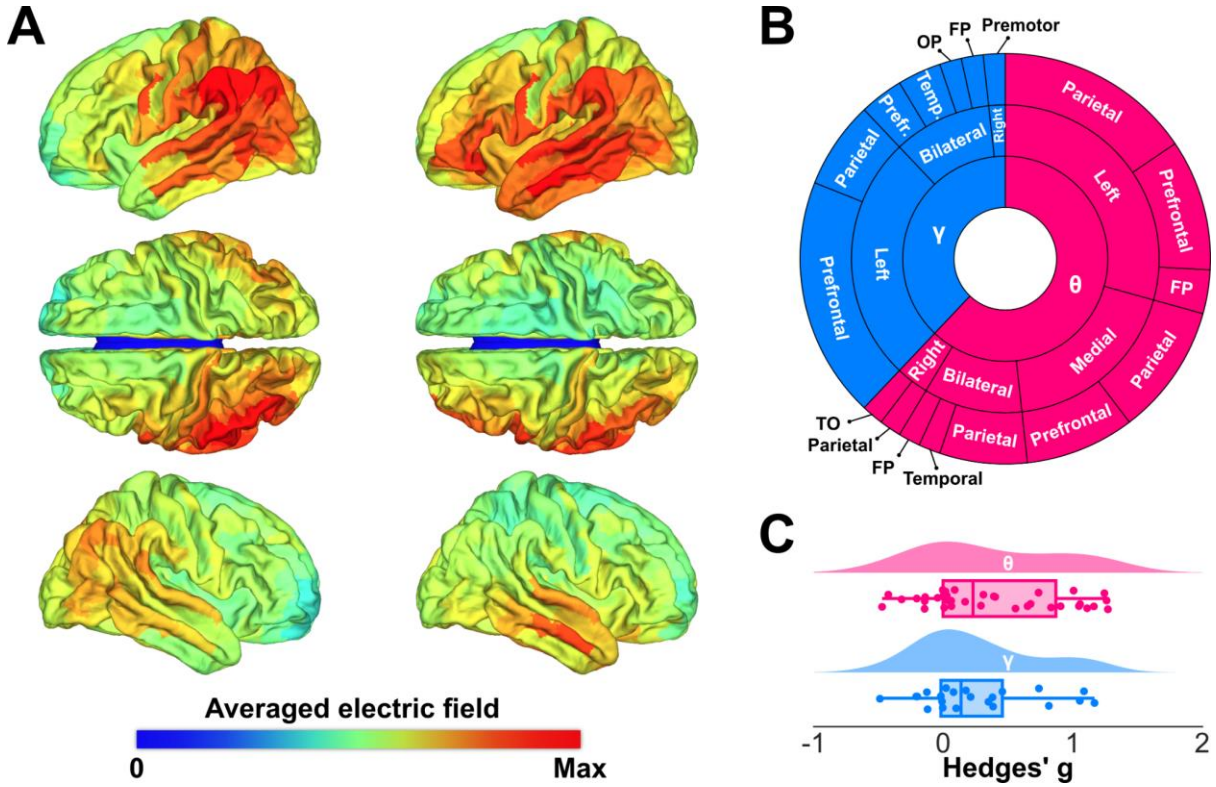

Figure 1. *A) Electric field strength averaged over all montages used in the selected articles, split for theta and gamma stimulation. Warm colors, where electric fields were strong on average, reflect regions commonly targeted across studies, while cold colors, where electric fields were weak on average, indicate regions less commonly targeted. B) A sunburst plot providing a global reflection of montages used across studies. FP: frontoparietal, OP: occipitoparietal, TO: Temporo-occipital. C) Raincloud distribution of effect sizes for theta and gamma tACS studies, showing an overall cumulative effect. Box plot limits correspond to the 25th and 75th percentiles, with the center line representing the median, and whiskers representing 1.5x interquartile range.*

Results

In total 20 articles were identified for inclusion in the present meta-modeling analysis[25–28,33,56–70]. The analysis was split for studies that targeted theta oscillations (3-8 Hz) and gamma oscillations (30-200 Hz). For theta tACS studies, N=36, and for gamma tACS studies, N=22 effect sizes were obtained (Figure 1C). In three papers, tACS frequencies other than theta and gamma were studied, which were not included in our analysis (Supplementary Table 1). Since studies used various montages, we first aimed to get a sense of the general distribution of electric fields (Figure 1B). As such, we averaged electric fields across all studies (Figure 1A). For both frequencies, the simulations indicated widespread distribution across the brain, which is in line with electrodes being placed on frontal, temporal and occipito-parietal regions. However, for theta the averaged electric field was stronger at the left parietal cortex, whereas for gamma it was stronger for left frontal, temporal and parietal regions. This reflects a bias in the literature of preferentially targeting the left hemisphere.

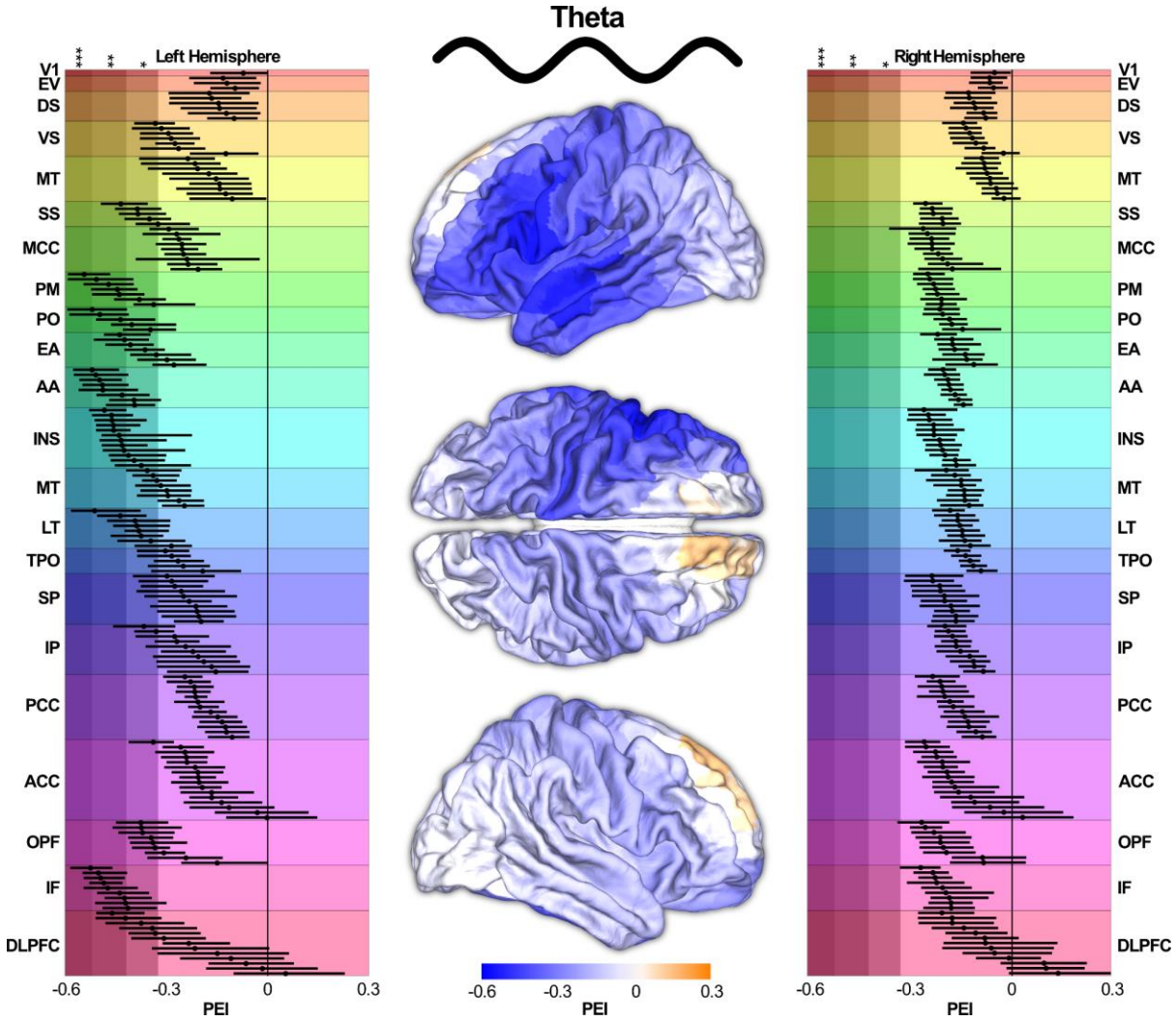

Figure 2. *Distribution of PEI values across the brain related to theta tACS. Exact PEI values for all 360 regions, categorized into 22 larger regions (Huang et al., 2022), are reflected on the left and right.*

Theta tACS on LTM

For the theta tACS we found no regions that were related to improvement of LTM, with a maximum of PEI = 0.052 ($p = 0.761$; right area 8B). In contrast, left frontal and temporal regions showed a negative linear association between electric field strength and LTM performance ($p<0.001$: N=2; $0.001<p<0.01$: N=34; $0.01<p<0.05$: N=39). Results are shown in Figure 2 and Table 1. Strongest associations were found in region 6r (PEI = -0.545, $p = 5.7e-4$) and 44 (PEI = -0.526, $p = 9.6e-4$) of the HCP-MMP atlas.

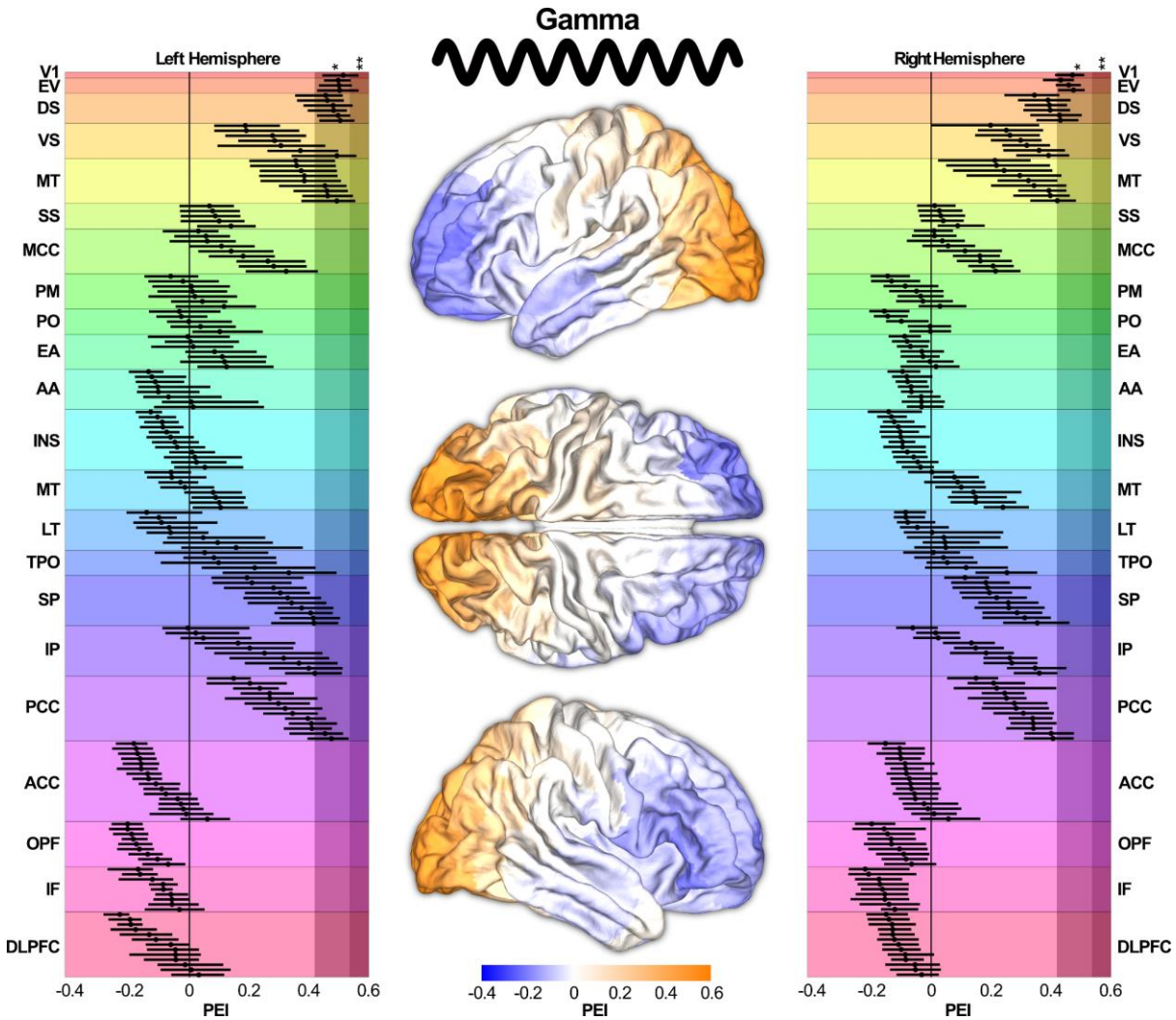

***Figure 3**. Distribution of PEI values across the brain related to gamma tACS. Exact PEI values for all 360 regions, categorized into 22 larger regions (Huang et al., 2022), are reflected on the left and right.*

Gamma tACS on LTM

For gamma tACS there was tentative evidence for bilateral occipital and parietal regions being related to improved LTM ($p<0.05$: N=24). The regions with the strongest associations were V1 (PEI = 0.514, p = 0.014) and V3A (PEI = 0.504, p = 0.016). No regions were found with a significant negative association between electric field magnitude and LTM performance, with a minimum of PEI = -0.232 (p = 0.297, left area anterior 9-46v). Results are shown in Figure 3 and Table 2.

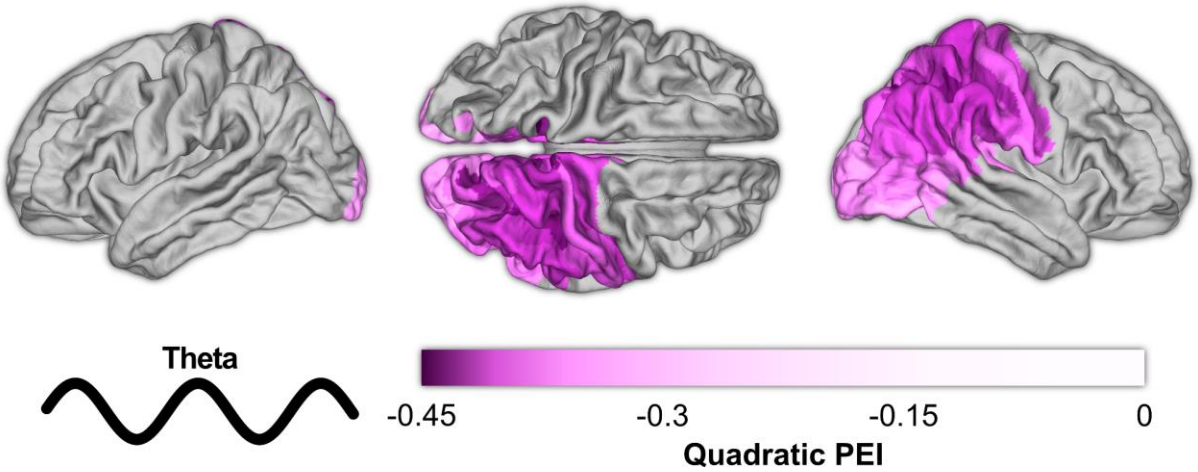

Figure 4. *Distribution of PEI_{QUAD} values across the brain related to theta tACS, reflecting a quadratic relationship between electric field strength and behavioral performance.*

Quadratic associations between electric field magnitude and LTM

In an exploratory analysis we investigated whether regions show a quadratic relationship between electric field and effect size (Figure 4). For theta tACS, we found that a quadratic relationship explained the variance better in 92 out of the 360 regions (i.e., a linear relationship explained more variance in the remaining 268 regions). This quadratic effect was observed in right occipito-parietal region. These 92 regions corresponded to a significant negative quadratic PEI, ranging between PEI_{QUAD} = -0.353 ($p = 0.035$) and PEI_{QUAD} = -0.468 ($p = 0.007$). This negative relationship indicates that mid-level electric field strengths had a positive effect on LTM performance, whereas low and high electric field strengths did not. No significant positive quadratic PEI values were found. For gamma stimulation, no regions were identified where a quadratic fit was superior to a linear fit.

Discussion

We aimed to summarize published LTM-tACS studies to date by correlating tACS-induced electrical fields in brain models with corresponding changes in LTM performance. As a result, we found that within the theta frequency range, no regions showed a significant linear relationship that improved memory performance, but modulation of the left frontal and temporal lobes led to worse performance across studies. Exploring quadratic relationships, we found that theta over the right parietal cortex improves memory at moderate (but not high and low) electric field strengths. For gamma frequencies, parieto-occipital areas were associated with better performance, whereas frontal areas were associated with worse performance.

In contrast to our expectations, no clear linear positive relationship was found between theta stimulation and LTM performance. Only the dorsomedial prefrontal cortex showed a positive association. And while theta in the medial PFC has been linked to LTM in animal studies[12,71–73], our results provide little support for this in humans. In contrast, and against our expectations, we found a negative association between LTM performance and electric field strength in left lateral prefrontal and temporal areas. The lateral prefrontal cortex is often associated with general cognitive performance and control, and various studies have at least suggested a potential role in LTM[25,74–77]. The temporal lobe includes and is connected to the hippocampus, which is often referred to as the main hub for LTM[78–81]. Within the hippocampus and medial temporal lobe, theta is a dominant oscillation[19,82–84]. Therefore, we hypothesized a

positive PEI for this region. One possible explanation is that the exogenous stimulation in the collected studies did not entrain but rather disrupted endogenous theta frequency or phase coupling. While tACS is generally thought to entrain regions and thereby strengthen endogenous oscillations[22], various studies have emphasized that this may depend on specific circumstances[32]. For instance, several studies investigate in-phase vs anti-phase tACS, suggesting that in-phase stimulation is more likely to increase synchronization between regions[85–89]. Phase of the endogenous oscillations also matters. For instance, by using an amplitude-modulated tACS design and sophisticated artifact cleaning methods, Haslacher et al[90] were able to record EEG while tACS is applied in a working memory task. They found that working memory depended on the phase lag between exogenous and endogenous theta oscillations. While this study looked at a different memory modality, it demonstrates the importance of phase alignment when aiming to modulate cognitive performance. Besides phase, recent studies have highlighted the importance of tACS intensity[52,53]. Specifically, lower intensities are more likely to decrease naturally occurring regional synchronization, rather than entrain a region. Furthermore, entrainment effects follow an Arnold's tongue pattern, with the strongest entrainment occurring for stimulation frequencies that are close to endogenous rhythms[91,92]. This emphasizes the importance of personalized stimulation frequencies, which many of the here included studies did not apply[47].

While we did not find any linear relationship between theta and LTM performance, when performing an additional analysis investigating a quadratic relationship, we found that this better explained the variance in 92 regions. Specifically, we found a significant negative quadratic effect in right parietal regions. In this case, a negative quadratic association reflects that the relation between electric field strength and LTM performance follows an inverted U pattern. This suggests that parietal theta stimulation with moderate, but not high, electric field strength was related to improved LTM performance. Indeed, various studies have demonstrated a nonlinear relationship between tACS intensity and neurophysiological and behavioral changes[51,54,55]. Wansbrough et al[55] demonstrated frequency-specific increase in EEG coherence after 0.5 mA tACS, while 1 or 1.5 mA tACS decreased coherence. On a behavioral level, Hsu et al[54] showed that 1 mA, but not 2 mA theta-tACS improve cognitive performance in patients with multiple sclerosis. Such inverted U relations have also been observed for other brain stimulation applications[93]. For example, Jamil et al[94] showed stronger after effects of motor cortical transcranial direct current stimulation after 1 mA, compared to sham and 2 mA stimulation. Indeed, various studies have proposed the idea of the brain as a homeostatic system, where modulation effects depend on the initial state of the brain[95–98].

For gamma tACS, we found that parieto-occipital regions were most strongly related to improvements in LTM. Indeed, studies have suggested that visual areas may serve as a storage or reactivation site for visual memory representations. For example, imaging work shows that visual memory traces may be maintained in the visual cortex[99–102]. Furthermore, gamma oscillations in particular have been related to sensory memory information[16,102,103]. On the other hand, gamma oscillations in the parieto-occipital cortex may reflect domain-general attentional mechanisms that support robust encoding and consolidation of memory by enhancing the binding of information and coordinating large-scale networks[104–110]. Previously, we found that gamma tACS of similar posterior regions enhances working memory performance[35], suggesting that parieto-occipital gamma is not exclusively related to LTM. Rather, it may reflect a broader mechanism supporting cognitive operations across memory timescales[14]. In sensory cortices, gamma oscillations have been linked to attentional selection

329 and feature binding, coordinating local neuronal ensembles to integrate information into
330 coherent representations[105,111,112]. Thus, gamma tACS over parieto-occipital areas may
331 facilitate long-term memory formation indirectly, by enhancing attentional and integrative
332 processes in visual regions that support effective encoding and consolidation. Whether
333 gamma tACS over the parietal cortex improves the sensory-mnemonic trace itself or improves
334 the attentional processes cannot be deduced from our results. Nevertheless, our results
335 suggest that stimulation of these regions most likely improves LTM performance.
336
337 Some considerations should be made when interpreting the results of the present study. First,
338 the included studies used a variety of tasks, stimuli, and sensory modalities. As such, we
339 cannot make any conclusions about specific memory domains. Rather, the PEI maps could
340 reflect improvement in domain-general LTM. Furthermore, while the results were split by
341 frequency, we pooled across different retrieval processes (recognition or recall), task
342 modalities (e.g., words, faces, or images), and stimulation timings (stimulation during
343 encoding, during retrieval, during both or offline). While it would be potentially interesting to
344 split by these factors, the limited sample of 20 studies does not allow for reliable subfactor
345 analyses. As such, more studies are required to explore the role of theta and gamma tACS in
346 different methodological approaches. Second, given the reliance on existing data, not all
347 potential montages have been explored. The PEI estimates rely on variability in electric fields
348 and capture effects within these commonly stimulated areas, while regions rarely or never
349 targeted should be interpreted with caution. The regions affected by the collected montages
350 were rather evenly distributed across the brain. Nonetheless, there was some bias towards
351 the temporoparietal areas and toward left hemispheric stimulation. Although such spatial bias
352 could influence the results, the lack of overlap between the average electric field and PEI maps
353 hints that any such effects were likely limited. Finally, it is important to note that the results
354 identify regions of interest based on the LTM-tACS studies conducted to date, not an exclusive
355 map of regions essential for memory per se. Various regions might be crucial for LTM
356 processing that are not susceptible to tACS-related improvements. Relatedly, since tACS
357 targets primarily cortical regions, we can draw no conclusion about the causal influence of
358 subcortical oscillations on LTM, for instance, those originating from hippocampal regions.
359
360 In conclusion, we illustrate the potential of noninvasive brain stimulation to modulate LTM and
361 shed light on the causal role of theta and gamma oscillations. As such, we find that tACS-
362 related improvement to LTM is location and frequency-specific. Additionally, tACS-induced
363 cognitive effects may not always scale linearly with intensity. Importantly, more studies are
364 required to explore specific aspects of LTM, including different modalities and various methods
365 of probing LTM. Nevertheless, we hope that these results provide a guide for future
366 fundamental, translational, and therapeutic studies aimed at modulating memory.
367
368 **Conflicts of interest**
369 The authors report no conflict of interests.
370
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374
375 **Author contributions**

DC: Data curation, Formal analysis, Methodology, Writing - original draft. MW: Conceptualization, Formal analysis, Funding acquisition, Methodology, Supervision, Visualization, Writing - review & editing

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Supplementary Table 1. Overview of studies using tACS at frequencies outside of the theta or gamma range (not included in the meta-analysis)

Reference	Montage	Freq. (Hz)	Intensity (mA)	Task	Time between encoding and retrieval	Hedges' g
Luckey et al. 2022	Bilateral C2 dermatome	40	3	word association task	7 days	0.17
Shtoots et al., 2024	Fz, AF4/AF3/FC2/FC1	16	1.5	delayed recall, pictures	2 hours	0.06
	Fz, AF4/AF3/FC2/FC1	16	1.5	delayed recall, pictures	1 day	0.08
	Fz, AF4/AF3/FC2/FC1	16	1.5	delayed recall, pictures	7 day	0.08
Shtoots et al., 2025	Chin, P1/P2/P3/P4	16	1.5	multiple choice exam, video	20 min	0.14
	Chin, P1/P2/P3/P4	16	1.5	multiple choice exam, video	1 day	0.12
	Chin, P1/P2/P3/P4	16	1.5	multiple choice exam, video	7 day	0.29
	P3, C3/TP7/Pz/O1	16	1.5	multiple choice exam, video	20 min	0.16
	P3, C3/TP7/Pz/O1	16	1.5	multiple choice exam, video	1 day	0.14
	P3, C3/TP7/Pz/O1	16	1.5	multiple choice exam, video	7 day	0.17
	Fz, AF4/AF3/FC2/FC1	16	1.5	multiple choice exam, video	20 min	0.10
	Fz, AF4/AF3/FC2/FC1	16	1.5	multiple choice exam, video	1 day	0.09
	Fz, AF4/AF3/FC2/FC1	16	1.5	multiple choice exam, video	7 day	-0.12