1 **Mapping long-term memory modulation with transcranial alternating current**
2 **stimulation**
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5 Running title: Mapping long-term memory
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Abstract

Background: Long-term memory (LTM), which is the ability to retain information over a long period of time, is governed by neural oscillations in various parts of the cerebral cortex. To investigate the relationship between oscillations and memory performance, transcranial alternating current stimulation (tACS) has been used to modulate LTM. However, due to the variability in stimulation parameters and locations, no clear picture has arisen on where tACS needs to be applied to improve LTM.

Methods: We collected behavioral data from 20 studies (58 effect sizes) and computationally modeled the corresponding brain electric fields based on each study's unique tACS parameters. As a result, we generated a map of performance–electric field index (PEI) values using linear and quadratic fits.

Results: Theta-tACS showed no regions with a positive linear association with LTM. However, left lateral prefrontal and temporal areas exhibited negative associations, meaning that theta stimulation of that region led to decreased LTM performance. A quadratic analysis revealed a U-shaped relation in the medial temporal and ventromedial prefrontal cortex, suggesting improved memory at low and high, but not moderate, electric field strength values. Gamma-tACS showed positive linear associations in parieto-occipital cortex and negative ones in frontal regions. For gamma, we found no regions that expressed a quadratic relationship.

Conclusion: These findings indicate that LTM-relevant tACS effects are frequency- and site-specific and potentially nonlinear with respect to intensity. Integrating meta-analytic effect sizes with individualized field estimates provides a brain-wide framework for identifying targets of memory modulation and for guiding future fundamental and translational research.

Keywords: Transcranial Alternating Current Stimulation; Long-term Memory; Meta-analysis; Electric Field Modeling; Neural oscillations

Introduction

The ability to retain information from hours, days, weeks, or even months ago is one of the hallmarks of the brain[1]. Besides the importance of gaining a fundamental understanding of the underlying brain mechanisms, long-term memory (LTM) studies are critical for further expanding the treatment options for memory-related deficits, such as Alzheimer's disease or traumatic brain injury[2,3]. In rodent models, memory is most commonly studied in subcortical areas, including the hippocampus and the amygdala[4–6]. However, human studies tend to focus on various cortical regions involved in processing and retaining information, including prefrontal, parietal, and temporal structures [7–12]. Furthermore, within these regions, particular neural oscillations, such as theta (3-8 Hz) and gamma (30-200 Hz), have been highlighted through their association with encoding and retrieval of memory[13–15].

Previous studies have investigated the role of oscillations using neurophysiological recordings. Osipova et al[16] engaged their participants in a picture recognition task while magnetoencephalographic (MEG) data were recorded. They found higher theta and gamma power both during encoding when the picture was subsequently remembered (subsequent memory effect) and during retrieval, when distinguishing old pictures from new. Furthermore, intracranial recordings from epilepsy patients showed a similar pattern, with increases in theta and gamma power over several cortical regions for subsequent memory effects[17–19]. In contrast, Hanouneh et al[20] showed that theta power in prefrontal regions was negatively correlated with LTM retrieval. However, Scholz et al[21] showed that theta power is positively associated with memory encoding.

Given the correlational nature and variability in results of the studies using electrophysiological techniques, others have used neuromodulation methods to pinpoint regions that causally relate to memory performance[22–24]. One particular technique suited to study neural rhythms is transcranial alternating current stimulation (tACS) and various studies have used it to alter cortical oscillations during memory tasks[25–28]. By applying a sinusoidal low-intensity current to the scalp, tACS has been shown to entrain neural spiking, which can result in a modulation of endogenous oscillatory activity[29,30]. Besides these neurophysiological effects, various studies have shown that tACS is able to modulate human behavior and cognition[25,31,32]. The rationale is that the tACS-induced entrainment of neural oscillations is directly related to changes in behavioral performance. As an example, long-term face recognition was improved by applying theta tACS to the right posterior parietal region during encoding[33]. On the other hand, Manippa et al[26] found reduced LTM performance following gamma tACS over bilateral temporal areas.

In accordance with the breadth of results in MRI and EEG studies, tACS has been applied in LTM experiments at various cortical locations and frequencies. Given the variety in parameters and protocols, a classic meta-analytic approach is suboptimal to summarize the efficacy of tACS, nor to identify core functional regions of LTM. By integrating meta-analytic results with electric field (E-field) modeling, this limitation can be overcome[34–37]. Using SimNIBS software, tACS-induced E-fields can be estimated based on a particular stimulation location and intensity[38]. By correlating the E-field distributions of different studies with their corresponding behavioral effect sizes (on LTM in this case), a meta-analytic brain map is generated that displays where tACS leads to increased, decreased, or no change in task performance[35].

104 In the present study, we leverage the meta-modeling approach to summarize the effects of
105 tACS on LTM. Thereby, we identify regions where neural oscillations in a given frequency
106 are directly related to memory performance. Altogether, these results aim to complement
107 previous research on cortical oscillations in LTM and point out cortical regions of interest for
108 LTM research.
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Figure 1. *PRISMA overview of included studies.*

Methods
Sample
We collected effect sizes, expressed in Hedges' g from available literature. The data was
obtained from articles published in peer-reviewed journals, pre-prints, and published theses,
by searching through PubMed, Web of Science, ProQuest (Dissertations and Theses),
BioRxiv and PsycINFO databases. The search was conducted in general accordance with
the PRISMA guidelines[39]. First, articles were identified using the following search terms:

("tACS" OR "transcranial alternating current stimulation") AND ("memory"). After removal of
duplicates, the texts underwent abstract and full-text screening. Inclusion of studies in our
modeling is based on the following criteria: I) Articles are written in English, II) Full-text is
available to the researchers, III) manuscripts allowed for extraction of effect size (based on
mean and standard deviation) from text, tables, or figures, IV) the study used a control
condition (e.g., placebo) to which active stimulation can be compared, V) the study was
conducted on a healthy adult population (>= 18 years old), VI) tACS applied online or offline,
but not during sleep, VII) long-term memory assessed explicitly. For the criteria, we rely on a
broad definition of long-term memory as information retrieved from the past that does not
rely on active maintenance[2]. A preliminary search suggested that 15-25 articles could be
eligible, suggesting that enough data can be collected to perform our meta-modeling
analyses. In total, the final search (Figure 1) yielded 20 articles and 58 unique effect sizes
(note that one study typically has multiple outcome measures). Across all studies n = 1210
healthy volunteers were included between the ages of 18-77. Since previously published
data were used, no ethical approval was obtained.
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Effect size calculation
The standardized effect sizes were expressed as Hedges' g values[40]. Hedges' g values
express the ratio between differences in effects and the variability, similar to Cohen's d
values[41], with the addition of a correction factor for small sample sizes. If Hedges' g values
were reported, they were directly taken from the article. Alternatively, if the article provided
the Cohen's d value, the correction factor was applied to calculate Hedges' g. If no effect
size measures were directly reported, the Hedges' g was calculated based on reported
averages and standard deviations or those estimated from graphs. All effect sizes used in
this analysis reflect the difference between an active stimulation condition and a sham
control. As such, positive g values reflect improved memory performance in active tACS
conditions compared to sham, while negative g values indicate worsened memory
performance in active tACS conditions compared to sham.
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Electric field modeling
E-field simulations were performed on 50 realistic head models (age range 22-35, 22
females). The head models were generated based on data from the Human Connectome
Project (HCP) S1200[42]. Quality and suitability for E-field modeling were assessed
previously[43]. Each head model consists of 6 biological tissues, namely the skin, skull,
cerebrospinal fluid, eyes, gray matter and white matter. For each tissue standard
conductivity values were used ($\sigma_{skull} = 0.01$ S/m, $\sigma_{skin} = 0.465$ S/m,
$\sigma_{CSF} = 1.654$ S/m, $\sigma_{graymatter} = 0.275$ S/m, and $\sigma_{whitematter} = 0.126$ S/m)[44,45].
Electrode location, orientation, and material were gathered from the articles and used for E-
field modeling in SimNIBS 4.1[38]. For the purpose of this study, we extracted the induced E-
fields from the gray matter, as this reflects the tissue at which tACS most likely induces
functional changes[46,47]. In order to compare and average between head models, all E-field
simulations were transformed into the normalized FreeSurver average (fsavg) standard
brain. Importantly, by first performing simulations in the individual head models and then
transforming them into fsavg space (rather than directly performing electric-field simulations
in fsavg models), individual variability is still accounted for.
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Calculation of the performance-electric field index

To relate different elements of fsavg model to functional brain regions, each element was
categorized following the Human Connectome Project multimodal parcellation (HCP-MP)
atlas[48,49]. This atlas parcellates the brain models into 360 function regions (180 per
hemisphere). Given that we found 36 and 22 outcome measures for theta and gamma,
respectively, and 360 functional regions, a 36 x 360 matrix and a 22 x 360 matrix of E-field
values are obtained. These matrices are subsequently correlated with a vector of Hedges' g
values for each row of the matrix (i.e., for each functional region), resulting in two 1 x 360
vectors that represents the correlation between E-fields and tACS-induced performance
changes per frequency[34–37]. We refer to these values as the performance-electric field index
(PEI). Besides this, we report the uncorrected p-values. Note that due to the nature of meta-
analytic datasets, no a priori power analysis was performed, and the number of data points
depends on the available literature. As such, the exact p-value, and hence the optimal way
to correct for multiple comparisons, is somewhat arbitrary. Therefore, we opted to report
uncorrected p-values and visually represent them as $p < 0.05$ (*), $p < 0.01$ (**), and $p < 0.001$
(***). For visualization, we categorized the 360 HCP-MP atlas region into 22 larger regions[50].
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In addition to the linear correlation analysis, we performed an exploratory analysis testing for
a potential quadratic relationship between E-field strength and performance. This analysis
was performed as several studies have shown that the effects of tACS follow a U-shape[51–53]
or an inverted U-shape [54,55]. For each cortical region, we fit a linear ($y = \beta_0 + \beta_1 x$) and a
quadratic regression model ($y = \beta_0 + \beta_1 x + \beta_2 x^2$), with the behavioral effect size (Hedges' g)
as the dependent variable and regional E-field magnitude as the predictor. For both linear
and quadratic models, a correlation value was defined as the signed square root of R-
squared, with the sign determined by the regression values being positive or negative. For
each region, we determined the better-fitting model (linear or quadratic) based on adjusted
R-squared. Across 50 head models, results were averaged per region. If more than 50% of
the head models yielded a better fit for a quadratic regression in a particular region, the
quadratic correlation values were averaged. We refer to this value as the PEI_{QUAD}, where
positive and negative values correspond to a U-shaped and an inverted U-shaped
relationship between E-field strength and performance, respectively.
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Table 1. Overview of studies using theta tACS included in the meta-analysis.

Reference	Montage	Freq. (Hz)	Intensity (mA)	Task	Time between encoding and retrieval	Hedges' g
Alekseichuk et al., 2020	P4, T8/C2/CP1/Oz	4	3	face recognition	20 min	0.31
	P3, T7/C1/CP2/Oz	4	3	face recognition	20 min	0.06
Chantrel et al., 2021	F3, left wrist	6	1.5	word recognition	90 min	-0.32
	F3, left wrist	6	1.5	word recognition	7 days	-0.15
Ergo et al., 2020	FCz, neck	6	2	word association task	Immediate	-0.21
Grover et al., 2022	FP1/F1/FC3/F5/AF7/Afz, Fz/AF3/cheek	4	1.58	delayed recall, words	Immediate	0.01
	C3/T7/CP1/FC5/TP7FT7/PO7/cheek, CP5	4	1.58	delayed recall, words	Immediate	0.06
	C3/T7/CP1/FC5/TP7FT7/PO7/cheek, CP5	4	1.58	delayed recall, words	1 month	0.17
Klink et al., 2020	Intersection of T3/F3/C3/F7, rSOR	5	1	face-occupation task	20 min	-0.14

Reference	Montage	Freq. (Hz)	Intensity (mA)	Task	Time between encoding and	Hedges' g
	Intersection of T3/F3/C3/F7, rSOR	5	1	face-occupation task	1 day	0.03
Komissarenko et al., 2025	F7, P7	5.5	1	word association recognition	1 min	-0.04
	F7, P7	5.5	1	word association recognition	4 days	-0.14
Lang et al., 2019	right fusiform 4x1	6	4	face-scene association	online	0.56
Meng et al., 2021	P3, ring surround	6	2	face-scene task, pictures	5 min	-0.42
Murray et al., 2023	T3, T4	6	1.5	delayed recall, words	20 sec	-0.47
Shtoots et al., 2024	Chin, P1/P2/P3/P4	3	1.5	delayed recall, pictures	2 hours	0.29
	Chin, P1/P2/P3/P4	3	1.5	delayed recall, pictures	1 day	0.39
	Chin, P1/P2/P3/P4	3	1.5	delayed recall, pictures	7 day	0.4
	Fz, AF4/AF3/FC2/FC1	3	1.5	delayed recall, pictures	2 hours	1.11
	Fz, AF4/AF3/FC2/FC1	3	1.5	delayed recall, pictures	1 day	1.27
	Fz, AF4/AF3/FC2/FC1	3	1.5	delayed recall, pictures	7 day	1.26
Shtoots et al., 2025	Chin, P1/P2/P3/P4	3	1.5	multiple choice exam, video	20 min	1.05
	Chin, P1/P2/P3/P4	3	1.5	multiple choice exam, video	1 day	0.73
	Chin, P1/P2/P3/P4	3	1.5	multiple choice exam, video	7 day	0.65
	P3, C3/TP7/Pz/O1	3	1.5	multiple choice exam, video	20 min	1.24
	P3, C3/TP7/Pz/O1	3	1.5	multiple choice exam, video	1 day	1.16
	P3, C3/TP7/Pz/O1	3	1.5	multiple choice exam, video	7 day	1.01
	Fz, AF4/AF3/FC2/FC1	3	1.5	multiple choice exam, video	20 min	0.67
	Fz, AF4/AF3/FC2/FC1	3	1.5	multiple choice exam, video	1 day	0.83
	Fz, AF4/AF3/FC2/FC1	3	1.5	multiple choice exam, video	7 day	0.91
Varastegan et al., 2022	FPz, Oz	6	2	delayed recall, words	20 min	1.06
Wynn et al., 2024	AF4/P5, Cz	4	2	word recognition	15 min	0.09
Wynn et al., 2020	P7/P8, Cz	3.5	2	word recognition	7 min	0.03
	P7/P8, Cz	3.5	2	screen location recognition	7 min	0.00
	P7/P8, Cz	8	2	word recognition	7 min	0.02
	P7/P8, Cz	8	2	screen location recognition	7 min	0.00

Table 2. Overview of studies using gamma tACS included in the meta-analysis.

Reference	Montage	Freq. (Hz)	Intensity (mA)	Task	Time between encoding and	Hedges' g

					retrieval	
Ambrus et al., 2015	F3/F4, left/right mastoid	140	1	cued recall, words	10 min	-0.20
	F3/F4, left/right mastoid	140	1	cued recall, words	12 hours	0.00
Chantrel et al., 2021	F3, left wrist	60	1.5	word recognition	90 min	-0.21
	F3, left wrist	60	1.5	word recognition	7 days	-0.49
	C4, left wrist	60	1.5	word recognition	7 days	-0.12
Grover et al., 2022	FP1/F1/FC3/F5/AF7/Afz, Fz/AF3/cheek	60	1.58	delayed recall, words	Immediate	-0.01
	FP1/F1/FC3/F5/AF7/Afz, Fz/AF3/cheek	60	1.58	delayed recall, words	1 month	0.17
	C3/T7/CP1/FC5/TP7FT7/PO7/cheek, CP5	60	1.58	delayed recall, words	Immediate	-0.02
Javadi et al., 2017	F3, left wrist	60	1.5	word recognition	1.5 hours	0.38
	F3, left wrist	60	1.5	word recognition	1.5 hours	0.46
	F3, left wrist	60	1.5	word recognition	1.5 hours	0.02
	F3, left wrist	60	1.5	word recognition	1.5 hours	0.38
Luckey et al., 2022	Bilateral C2 dermatome	40	3	word association task	7 days	1.05
Manippa et al., 2024	T7, T8	40	2	delayed recall, words	4 min	0.08
	T7, T8	60	2	delayed recall, words	4 min	-0.13
Nomura et al., 2019	F3, left arm	60	1.5	word recognition	Immediate	0.21
	F3, left arm	60	1.5	word recognition	1 day	0.74
	F3, left arm	60	1.5	word recognition	6 days	1.17
Sun et al., 2025	P3, right deltoid	60	1.5	cued recall, words	4 min	0.35
	P3, right deltoid	60	1.5	cued recall, words	7 days	0.81
	P3, right deltoid	60	1.5	cued recall, words	28 days	1.09
Wynn et al., 2024	AF4/P5, Cz	50	2	word recognition	15 min	0.10

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201 **Results**

202 In total 20 articles were identified for inclusion in the present meta-modeling analysis[25–28,33,56–70]. The analysis was split for studies that targeted theta oscillations (3-8 Hz) and gamma oscillations (30-200 Hz). For theta tACS studies, N=36, and for gamma tACS studies, N=22 effect sizes were obtained (Figure 2C). In three papers, tACS frequencies other than theta and gamma were studied, which were not included in our analysis (Supplementary Table 1). Since studies used various montages, we first aimed to get a sense of the general distribution of E-fields (Figure 2B). As such, we averaged E-fields across all studies (Figure 2A). For both frequencies, the simulations indicated widespread distribution across the brain, which is in line with electrodes being placed on frontal, temporal and occipito-parietal regions. However, for theta the averaged E-field was stronger at the left parietal cortex, whereas for gamma it was stronger for left frontal, temporal and parietal regions. This reflects a bias in the literature of preferentially targeting the left hemisphere.

Figure 2. *A) E-field strength averaged over all montages used in the selected articles, split for theta and gamma stimulation. Warm colors, where E-fields were strong on average, reflect regions commonly targeted across studies, while cold colors, where E-fields were weak on average, indicate regions less commonly targeted. B) A sunburst plot providing a global reflection of montages used across studies. FP: frontoparietal, OP: occipitoparietal, TO: Temporo-occipital. C) Raincloud distribution of effect sizes for theta and gamma tACS studies, showing an overall cumulative effect. Box plot limits correspond to the 25th and 75th percentiles, with the center line representing the median, and whiskers representing 1.5x interquartile range. D) The distribution of tACS frequencies used in the included studies. E) Pie charts showing whether studies applied tACS during encoding, retrieval, both, or offline (between encoding and retrieval). F) Pie charts showing how stimuli were presented across studies, either visually, auditorily, or a combination of both. G) Pie charts showing the type of LTM that was investigated across studies.*

Across all included studies, a wide variety of study designs and tasks were used (Figure 2D-G). The majority of theta tACS studies used stimulation frequencies at the lower end of the theta range, with 75% of effect sizes from studies using a frequency ≤ 5.5 Hz. In those studies that applied gamma tACS, 60 Hz was the most common frequency (77.2%). For theta tACS studies, stimulation was either applied during encoding (30.6%), retrieval (25%), or offline (44.4%). For gamma tACS studies, stimulation was applied only during the task: During encoding (50%), retrieval (18.2%), or both (31.8%). Most studies used visual stimuli

(theta: 58.3%; gamma: 77.2%), while the remaining studies used auditory stimuli (theta:
11.1%; gamma: 22.8%), or a combination of both (theta: 30.5%). Furthermore, various LTM
task variations were used, including semantic memory, associative memory, free item recall,
and item recognition (Figure 2G). Semantic memory studies provided to-be-memorized
information that was subsequently quizzed. In studies using associative memory tasks,
stimuli were paired, and the association between these items had to be remembered. In free
recall tasks, the goal was to recall as many items from a given list as possible. In recognition
tasks, a set of stimuli was memorized, and during retrieval, a set of new and old items was
presented, with the goal of recognizing which items had been seen before. Given the wide
variety of designs, it was not possible to include these factors in the subsequent meta-
modeling analysis, as the small sample sizes would have yielded unreliable results.
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250 ***Figure 3***. *Distribution of PEI values across the brain related to theta tACS. Exact PEI values for all*
251 *360 regions, categorized into 22 larger regions (Huang et al., 2022; reflected by rainbow-colored*
252 *shading), are reflected on the left and right. Gray shading reflects levels of significance with light*
253 *shading p<0.05 (*), medium shading p<0.01 (**), and dark shading p<0.001 (***).*
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Theta tACS on LTM
For the theta tACS we found no regions where E-field strength showed a positive linear
relationship with LTM performance, with a maximum of PEI = 0.052 (p = 0.761; right area
8B; frontal eye field). In contrast, E-field strength in the left frontal and temporal regions

showed a negative linear association with LTM performance (p<0.001: N=2; 0.001<p<0.01:
N=34; 0.01<p<0.05: N=39). Results are shown in Figure 3 and Supplementary Table 2. The
strongest PEI values were found in regions 6r (PEI = -0.545, p <0.001) and 44 (PEI = -0.526,
p < 0.001) of the HCP-MMP atlas, corresponding to the posterior part of the dorsolateral
prefrontal and inferior frontal cortex, respectively.
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266 **Figure 4**. *Distribution of PEI values across the brain related to gamma tACS. Exact PEI values for all*
267 *360 regions, categorized into 22 larger regions (Huang et al., 2022; reflected by rainbow-colored*
268 *shading), are reflected on the left and right. Gray shading reflects levels of significance with light*
269 *shading p<0.05 (*), medium shading p<0.01 (**), and dark shading p<0.001 (***).*
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Gamma tACS on LTM
For gamma tACS there was tentative evidence for E-field strength in bilateral occipital and
parietal regions showing a positive linear relationship with LTM performance (p<0.05: N=24).
The regions with the strongest associations between E-field strength and Hedges' g were V1
(PEI = 0.514, p = 0.014) and V3A (PEI = 0.504, p = 0.016), in the visual cortex. No regions
were found where E-field strength showed a significant negative linear relationship with
performance, with a minimum of PEI = -0.232 (p = 0.297, left area anterior 9-46v;
dorsolateral prefrontal cortex). Results are shown in Figure 4 and Supplementary Table 3.
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Figure 5. Distribution of PEI_{QUAD} values across the brain related to theta tACS, reflecting a quadratic relationship between E-field strength and behavioral performance.

Quadratic associations between E-field magnitude and LTM

In an exploratory analysis we investigated whether regions show a quadratic relationship between E-field and effect size (Figure 5A). For theta tACS, we found that a quadratic curve explained the relationship between E-field strength and LTM performance better in 67 out of the 360 regions (i.e., a linear relationship explained more variance in the remaining 293 regions). This quadratic effect was observed in ventromedial prefrontal and medial temporal cortices. In all 67 regions a positive PEI was found ranging between $PEI_{QUAD} = 0.349$ (p = 0.039) and $PEI_{QUAD} = 0.584$ (p < 0.001). This positive relationship indicates that low and high E-field strength values had a positive effect on LTM performance, whereas medium E-field strength values did not. A visualization of this relationship is shown in Figure 5B, demonstrating the three regions with the highest PEI_{QUAD} values (Glasser region 47m, ventromedial prefrontal cortex, $PEI_{QUAD} = 0.584$; Glasser region PeEC, medial temporal cortex, $PEI_{QUAD} = 0.547$; and Glasser region PoI1, insular cortex, $PEI_{QUAD} = 0.542$). In these examples, it can be observed that at medium electric field strengths (≈0.05 to 0.1 mV/mm), tACS has no beneficial effect on LTM performance. However, at very small (<0.05 mV/mm) and large (>0.1 mV/mm) electric field strength values, there is. No significant negative quadratic PEI values were found. For gamma stimulation, no regions were identified where a quadratic fit was superior to a linear fit.

Discussion

We aimed to summarize published LTM-tACS studies to date by correlating tACS-induced electrical fields in brain models with corresponding changes in LTM performance. As a result, we found that within the theta frequency range, no regions showed a significant linear

relationship that improved memory performance, but modulation of the left frontal and
temporal lobes led to worse performance across studies. Exploring quadratic relationships,
we found that theta over the ventromedial prefrontal and medial temporal cortices improves
memory at low and high (but not moderate) E-field strength values. For gamma frequencies,
parieto-occipital areas were associated with better performance, whereas frontal areas were
associated with worse performance.
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In contrast to our expectations, no clear linear positive relationship was found between theta
stimulation and LTM performance. Only the dorsomedial prefrontal cortex showed a positive
association. And while theta in the medial PFC has been linked to LTM in animal studies[12,71–
73], our results provide little support for this in humans. In contrast, and against our
expectations, we found a negative association between LTM performance and E-field
strength in left lateral prefrontal and temporal areas. The lateral prefrontal cortex is often
associated with general cognitive performance and control, and various studies have at least
suggested a potential role in LTM[25,74–77]. The temporal lobe includes and is connected to the
hippocampus, which is often referred to as the main hub for LTM[78–81]. Within the
hippocampus and medial temporal lobe, theta is a dominant oscillation[19,82–84]. Therefore, we
hypothesized a positive PEI for this region. One possible explanation for this discrepancy is
that the exogenous stimulation in the collected studies did not entrain but rather disrupted
endogenous theta frequency or phase coupling. While tACS is generally thought to entrain
regions and thereby strengthen endogenous oscillations[22], various studies have emphasized
that this may depend on specific circumstances[32]. For instance, several studies investigate
in-phase vs anti-phase tACS, suggesting that in-phase stimulation is more likely to increase
synchronization between regions[85–89]. Phase of the endogenous oscillations also matters.
For instance, by using an amplitude-modulated tACS design and sophisticated artifact
cleaning methods, Haslacher et al[90] were able to record EEG while tACS is applied in a
working memory task. They found that working memory depended on the phase lag between
exogenous and endogenous theta oscillations. While this study looked at a different memory
modality, it demonstrates the importance of phase alignment when aiming to modulate
cognitive performance. Besides phase, recent studies have highlighted the importance of
tACS intensity[52,53]. Specifically, lower intensities are more likely to decrease naturally
occurring regional synchronization, rather than entrain a region. Furthermore, entrainment
effects follow an Arnold's tongue pattern, with the strongest entrainment occurring for
stimulation frequencies that are close to endogenous rhythms[91,92]. This emphasizes the
importance of personalized stimulation frequencies, which many of the here included studies
did not apply[47].
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While we did not find any linear relationship between theta and LTM performance, when
performing an additional analysis investigating a quadratic relationship, we found that this
better explained the variance in 67 regions. Specifically, we found a significant positive
quadratic effect in medial temporal and ventromedial prefrontal regions. In this case, a
positive quadratic association reflects that the relation between E-field strength and LTM
performance follows a U-shaped pattern. This suggests that parietal theta stimulation with
low and high, but not moderate, E-field strength values was related to improved LTM
performance. Indeed, various studies have demonstrated a nonlinear relationship between
tACS intensity and neurophysiological and behavioral changes[51,54,55]. The U-shaped
relationship between electric field strength and behavioral outcomes corresponds to
physiological studies in animals showing that tACS-induced entrainment also follows a U-

shape[52,93]. Krause et al[52] found that while 2 mA tACS entrains neural firing to the exogenous
current, 1 mA stimulation decreased entrainment compared to the natural entrainment to
endogenous rhythms. This potentially suggests that tACS 'makes things worse before it
makes things better'. Nevertheless, the present results are surprising as they suggest
improved LTM performance at electric field strength values < 0.05, which likely has a
negligible effect on the brain[94]. As such, these effect sizes are more likely explained by
factors unrelated to tACS, such as placebo-related or task-related learning effects.
Alternatively, it could reflect a limitation of our method, as it does not take into account
functional or structural connectivity between regions. For example, a region experiencing
weak local electric fields may be strongly connected to another region exposed to higher
field strengths, potentially leading to behavioral effects that the current method would not
capture. Overall, while these interpretations remain speculative, the present findings
highlight the importance of considering non-linear interactions between tACS and behavior. .
369
For gamma tACS, we found that parieto-occipital regions were most strongly related to
improvements in LTM. Indeed, studies have suggested that visual areas may serve as a
storage or reactivation site for visual memory representations. For example, imaging work
shows that visual memory traces may be maintained in the visual cortex[95–98]. Furthermore,
gamma oscillations in particular have been related to sensory memory information[16,98,99]. On
the other hand, gamma oscillations in the parieto-occipital cortex may reflect domain-general
attentional mechanisms that support robust encoding and consolidation of memory by
enhancing the binding of information and coordinating large-scale networks[100–106].
Previously, we found that gamma tACS of similar posterior regions enhances working
memory performance[35], suggesting that parieto-occipital gamma is not exclusively related to
LTM. Rather, it may reflect a broader mechanism supporting cognitive operations across
memory timescales[14]. In sensory cortices, gamma oscillations have been linked to
attentional selection and feature binding, coordinating local neuronal ensembles to integrate
information into coherent representations[101,107,108]. Thus, gamma tACS over parieto-occipital
areas may facilitate long-term memory formation indirectly, by enhancing attentional and
integrative processes in visual regions that support effective encoding and consolidation.
Whether gamma tACS over the parietal cortex improves the sensory-mnemonic trace itself
or improves the attentional processes cannot be deduced from our results. Nevertheless, our
results suggest that stimulation of these regions most likely improves LTM performance.
389
When interpreting the main results, the variability in experimental designs was not
considered a factor, as this would have been problematic with small sample sizes and would
have led to unreliable results. Our PEI maps, therefore, reflect domain-general LTM.
However, when interpreting our results, it is worth keeping these factors in mind. One such
factor to consider is the exact frequency of stimulation. In working memory research,
accumulating evidence suggests that stimulation at the lower range of theta may be
beneficial for item maintenance[109–111], although this observation likely also depends on the
stimulation region[35]. Within the included studies, only Wynn et al[62] compared low (3.5 Hz)
and high (8 Hz) theta. In their visual recognition memory task, they found that neither
stimulation frequency (applied over the parietal cortex) improved memory accuracy.
However, low theta stimulation significantly reduced participants' confidence in their memory
performance. Evidence from intracranial recordings in surgical patients has shown that both
low and high hippocampal theta power are positively related to spatial LTM performance[19].
Importantly, the majority of studies included in the present meta-analysis used low-frequency

theta stimulation (<5.5 Hz). In how far this affected the results is open to debate, but it does reflect the need for more high-theta tACS studies and comparisons between low and high theta. In our meta-analysis, variation in the gamma frequency band was limited, with most studies using 60 Hz stimulation. While this reduces variability within our meta-analysis, it also highlights the importance of exploring a larger variety of stimulation frequencies within the gamma range.

The second factor to consider is the timing of stimulation. Across the studies, tACS was applied during encoding, during retrieval, during both encoding and retrieval, or offline (between encoding and retrieval). As such, the stimulation served conceptually distinct purposes, namely memory formation, consolidation, and recollection. The cortical networks and oscillatory processes related to these memory phases only partially overlap[112], meaning that stimulation frequency and location need to be adjusted to each process. For instance, Shtoots and colleagues[27,68] applied offline theta tACS (during the consolidation period) to the dorsomedial prefrontal cortex to test the role of midline theta in memory consolidation. On the other hand, Javadi et al[57], who applied tACS during both encoding and retrieval, demonstrated the importance of matching stimulation frequencies for both periods, which is in line with the idea of context-dependent memory[113]. While speculative, it is possible that a specific memory phase is more susceptible to tACS than others. While our meta-analysis cannot answer this question, the different stimulation timings were represented by roughly equal numbers of effect sizes (Figure 2E), suggesting that our results are unlikely to be driven by a single factor.

A third factor that may influence the effect of tACS on LTM is the modality in which to-be-remembered stimuli are presented. Most studies used visual stimuli, with a minority of studies using auditory stimuli (or a combination of both). Other modalities, such as olfactory or tactile memory, were not investigated. This is a common bias for cognitive neuroscience in general, given the ease of computerized tasks[114]. We found gamma tACS over the occipitoparietal regions was positively correlated with improved LTM performance. A similar finding was previously observed for working memory[35]. More optimal visual processing, and thus increased occipital gamma, likely improves visual LTM performance. As such, it cannot be guaranteed that these results hold for other modalities.

A fourth factor to consider is the memory type. In other words, how participants had to remember information. Within our sample, some studies focused on the familiarity of items (e.g., "Have I seen this item before?"). Others targeted associative or semantic memory, requiring participants to retrieve relations between items or concepts embedded in a larger knowledge structure (e.g., "Did item X belong to item Y?"). This variety in forms of LTM is likely driven by different brain networks[112,115]. Furthermore, executive demands and cognitive control are likely to differ in associative memory tasks, compared to tasks with simple item recall or recognition[116]. Our results on theta tACS showed no significant regions positively associated with LTM performance. However, the regions showing a trend in this direction were in the prefrontal cortex. This pattern may be driven by studies employing tasks with higher cognitive demands, such as associative memory paradigms. Notably, the distribution of task types used in our sample was relatively balanced, making it unlikely that the overall results were dominated by a single form of memory. Nevertheless, future studies would benefit from directly comparing the effects of tACS across different forms of memory within the same experimental design.

452
Besides the above-mentioned factors some further considerations should be made when
interpreting the results of the present study. First, given the reliance on existing data, not all
potential montages have been explored. The PEI estimates rely on variability in E-fields and
capture effects within these commonly stimulated areas, while regions rarely or never
targeted should be interpreted with caution. The regions affected by the collected montages
were rather evenly distributed across the brain. Nonetheless, there was some bias towards
the temporoparietal areas and toward left hemispheric stimulation. Although such spatial
bias could influence the results, the lack of overlap between the average E-field and PEI
maps hints that any such effects were likely limited. Second, it is important to note that the
results identify regions of interest based on the LTM-tACS studies conducted to date, not an
exclusive map of regions essential for memory per se. Various regions might be crucial for
LTM processing that are not susceptible to tACS-related improvements. Relatedly, since
tACS targets primarily cortical regions, we can draw no conclusion about the causal
influence of subcortical oscillations on LTM, for instance, those originating from hippocampal
regions. Third, the present analyses were conducted using uncorrected p-values. This
choice reflects a trade-off between statistical conservatism and sensitivity that is inherent to
correlational meta-modeling approaches, which typically require large samples for stable
inference. In the context of tACS research, the available literature remains limited in both the
number of studies and outcome measures, constraining statistical power. Because the
sample size in such analyses is determined by the existing literature rather than by an a
priori design, conventional power calculations and standard multiple-comparison correction
procedures are difficult to apply. While this approach increases sensitivity to detect potential
effects, it also necessitates cautious interpretation of marginal findings. Fourth, electric field
strength values were estimated using a set of 50 head models from the HCP S1200 dataset
rather than participant-specific MRI data. This approach was chosen to incorporate realistic
inter-individual anatomical variability in the absence of access to individual-level imaging
data from the included studies. Nevertheless, this procedure constitutes an approximation,
as the modeled electric fields cannot capture the exact anatomical properties of participants
in the original experiments. Finally, as mentioned previously, our method does not consider
the structural or functional connectivity and may be addressed by future refinements of
electric field models
484
In conclusion, we illustrate the potential of noninvasive brain stimulation to modulate LTM
and shed light on the causal role of theta and gamma oscillations. As such, we find that
tACS-related improvement to LTM is location and frequency-specific. Additionally, tACS-
induced cognitive effects may not always scale linearly with intensity. Importantly, more
studies are required to explore specific aspects of LTM, including different modalities and
various methods of probing LTM. Nevertheless, we hope that these results provide a guide
for future fundamental, translational, and therapeutic studies aimed at modulating memory.
492

493 **Conflicts of interest**
494 The authors report no conflicts of interest.
495
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DC: Data curation, Formal analysis, Methodology, Writing - original draft. MW:
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504

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