Airflow Determines Natural Airborne Transmission of Tuberculosis in a Guinea Pig Model

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ABSTRACT

Tuberculosis (TB) spreads through the air when *Mycobacterium tuberculosis* (Mtb) passes from infected to susceptible hosts, yet the environmental, biophysical and microbial factors governing this process remain poorly understood. In the early twentieth century, Perla and Lurie used guinea pigs to demonstrate natural airborne transmission of Mtb, but such studies have not been revisited in the modern biosafety era. Here, we developed an aerodynamically-optimized guinea pig housing system that models natural, airborne, animal-to-animal Mtb transmission under biosafety level 3 (BSL-3) containment. Iterative engineering and particle transport experiments revealed that airflow is a critical determinant of transmission efficiency. Static housing and excessive unidirectional ventilation both eliminated transmission, whereas controlled, low-velocity airflow enabled aerosol particle retention and exposure of naïve animals. Under these optimized conditions, recipient guinea pigs converted their tuberculin skin tests above a defined positive threshold, developed Mtb-specific antibody responses, and exhibited pulmonary inflammation consistent with infection. These findings demonstrate that flow rates govern natural transmission of Mtb and provide a reproducible small-animal model for studying bacterial, host, and environmental factors that drive infectious spread. By reviving a century-old experimental paradigm with modern physics, engineering and immunologic tools, this work establishes a platform to dissect the mechanisms underlying airborne transmission of tuberculosis.

INTRODUCTION

Tuberculosis (TB), caused by *Mycobacterium tuberculosis* (Mtb) infection, remains one of the leading causes of infectious mortality worldwide (2024). Interrupting the

transmission cascade is essential to reducing global incidence, yet progress is hindered

by an incomplete understanding of the host, bacterial and environmental factors that

govern the spread of infection. Reliable animal models that recapitulate natural

transmission are needed to dissect these factors and to accelerate development of

transmission-blocking interventions and vaccines.

Guinea pigs have played a central role in the history of TB research (Donald et al.,

2018). In 1882, Robert Koch established their use as a model for TB pathogenesis,

noting that naïve animals housed near infected ones occasionally developed

"spontaneous" pulmonary disease (Koch, 1882; Koch, 1912). In the 1920s and 1930s,

David Perla and Max Lurie expanded on these observations, demonstrating that healthy

guinea pigs co-housed with infected animals developed bronchogenic tuberculosis, and

that transmission could occur even between animals housed in separate cages within

the same room (Lurie, 1930a; Lurie, 1930b; Lurie, 1930c; Perla, 1927a; Perla, 1927b).

These seminal studies provided the first experimental evidence for airborne

transmission of Mtb. Decades later, Riley, Wells, and Mills extended this concept to

humans, showing that air exhausted from TB wards could infect sentinel guinea pigs

(Riley, 2001; Riley et al., 1962; Riley et al., 1957; Wells, 1955; Wells et al., 1948).

Despite these pioneering efforts, little progress has been made over the past century

toward developing a controlled small-animal system for experimental TB transmission.

Recent studies using minipigs (Ramos et al., 2017) and ferrets (Gupta et al., 2022) have

demonstrated animal-to-animal transmission of Mtb, but these models require high

infectious doses and lack correlation with natural respiratory behaviors such as

coughing. The guinea pig remains an ideal species to model transmission: it is relatively

low-cost compared to other models, develops necrotizing granulomas similar to humans

(Orme and Ordway, 2016), harbors Mtb within its airways during infection (Podell et al.,

2014), and exhibits respiratory neurophysiology closely resembling that of humans

(Canning, 2008; Mazzone et al., 2005). While guinea pigs have long been used as

sentinels for human-to-animal transmission in air sampling studies (Dharmadhikari et

al., 2011; Nardell, 1999; Riley et al., 1962; Riley et al., 1957; Stoltz et al., 2025), a

modern system that supports natural guinea pig-to-guinea pig transmission via airborne

particles under biosafety level 3 (BSL-3) conditions has not been established.

A key step in Mtb transmission is the generation and survival of aerosolized, pathogen-

containing particles capable of reaching the alveoli of a new host. Respiratory

maneuvers such as coughing (Fennelly et al., 2012; Fennelly et al., 2004; Loudon and

Spohn, 1969; Tristao et al., 2025; Turner and Bothamley, 2015), sneezing (Duguid,

1946), singing (Loudon and Roberts, 1968; Mangura et al., 1998), and breathing

(Dinkele et al., 2022) all produce aerosols containing Mtb. Once expelled, these

particles are shaped by environmental factors such as desiccation, humidity, ventilation,

and settling (Bourouiba, 2021) that determine their persistence and infectivity (Brown et

al., 2025; Mishra et al., 2025; Singh et al., 2025). Modeling these processes in

experimental systems is particularly challenging under BSL-3 conditions, where high

ventilation rates designed for personnel safety can markedly reduce airborne particle

retention.

Here, we describe the development of a guinea pig housing system engineered for

natural Mtb transmission of Mtb. Through iterative transmission trials and particle

transport measurements, we identify airflow as a critical determinant of transmission

efficiency. Transmission attempts using static housing and strong unidirectional airflow

resulted in no detectable transmission, underscoring the critical role of cage design,

ventilation rates, flow physics, and particle residence time in facilitating Mtb

transmission. To address this, we modeled and tested the flow physics components of

the designs under both ambient and BSL3 negative-pressure conditions. These

experiments identified ventilation and cage design regimes that maximized aerosolized

pathogen-laden microdroplet retention and distribution to the recipient side, thereby

increasing the probability of successful host-to-host transmission. Using this refined

system, we demonstrate that naïve guinea pigs co-housed with infected donors but

separated by a permeable barrier mount Mtb-specific cellular and humoral immune

responses and develop pulmonary inflammation. This work revives a classical model of

airborne Mtb transmission with modern engineering precision, demonstrates that

exposure or proximity alone are not sufficient to mediate airborne Mtb transmission,

highlights the critical role of airflow and ventilation in transmission, and establishes a

reproducible platform for dissecting the biophysical, environmental, microbial and host

factors that drive the spread of Mtb.

RESULTS

Airflow is a critical driver of transmission

Because early transmission studies in guinea pigs were performed in cages with likely

static airflow (Lurie, 1930b), we hypothesized that a similar approach could serve as a

foundation for a modern experimental system. We therefore tested the first iteration of

our guinea pig transmission system (system 0) by co-housing naïve recipient guinea

pigs with Mtb-infected donors, separated by a perforated plexiglass barrier for 12

months (Fig. 1A, B). Infection of naïve animals was monitored bimonthly by tuberculin

skin testing (TST).

This initial design emphasized simplicity, low-cost and ease of access to system

components. We modified an existing static cage by inserting a plexiglass divider

containing large holes to separate donor and recipient animals (Fig. 1B). The cages

were housed on a metal shelving system located in the most negatively pressurized

room of our ABSL3 facility (relative negative pressure -0.06 WC). Because guinea pigs

are highly susceptible to progressive tuberculosis following low-dose infection (50-100

CFU) (Orme and Ordway, 2016), infected donors were replaced every 7-8 weeks to

maintain a constant infectious source. After 12 months of exposure, none of the

recipient animals converted their TSTs or showed clinical or histopathologic evidence of

infection, and no Mtb CFU were recovered at necropsy.

The absence of transmission under these conditions contrasted sharply with historical

reports from Perla and Lurie and suggested that modern biosafety engineering

constraints might fundamentally alter airflow compared to the open systems used a

century ago. In contemporary BSL-3 facilities, negative-pressure ventilation ensures

containment but may also disrupt airborne particle movement between animals. We

therefore reasoned that introducing controlled, unidirectional airflow from infected to

naïve compartments could facilitate transport of infectious aerosols.

To test this, we modified a commercially available guinea pig housing system

(Allentown, Inc.) to create "system 1" (Fig. 1C, D). The new design incorporated a

stainless-steel barrier perforated with two panels of holes positioned at the typical nose

and mouth height of an adult guinea pig. To establish unidirectional airflow, we blocked

the donor-side exhaust port (right) and the recipient-side supply ports (left) with rubber

caps (Fig. 1E). Smoke testing confirmed right-to-left airflow from the donor to the

recipient compartment (Fig. 1F, Suppl. Movie 1). Recipient animals were then exposed

to infected donors for 12 months under these unidirectional airflow conditions. Despite

these adjustments, no transmission occurred: all recipients remained TST-negative and

free of histopathologic or microbiologic evidence of infection.

These findings demonstrated that simply imposing unidirectional airflow was insufficient

to drive natural Mtb transmission. Instead, they highlighted the need for quantitative

optimization of airflow rate and associated particle retention to enable sustained

exposure of naïve animals to infectious aerosols generated by donor guinea pigs.

Airflow and cage design influence particle dynamics

The inability of systems 0 and 1 to support transmission suggested that airflow and

cage architecture critically influence the movement and retention of airborne particles.

We therefore undertook an iterative series of aerosol studies to define the parameters

that would permit infectious particle transport from donor to recipient compartments.

To test aerosolized particle transport, we connected prototype cages to a supply air line

on the donor side and an exhaust vacuum on the recipient side, allowing controlled

regulation of airflow within the system. To simulate infectious particles, we used a

particle generator to produce aerosols ranging from 0.8-7 µm and sampled air at three

locations: upstream (before entering the cage), within the donor compartment, and

within the recipient compartment (Fig. 2A). Particles were loaded for 1 hour to establish

155 steady-state size distribution (Suppl. Fig. 1A) and sampled three times for 20 seconds

156 totaling 1 minute at each position.

157 We first characterized particle behavior under ambient room pressure, beginning with

158 the earliest systems, 0 and 1. In system 0, which lacked directional airflow, we observed

159 marked particle loss from both donor and recipient compartments, particularly for

160 particles larger than 4 µm (Fig. 2B-C). System 1, operated with the manufacturer's

161 default airflow settings (8.8 L/min supply; 2.5 L/min exhaust), also showed significant

162 particle depletion (Fig. 2D-E). These findings indicated that the high ventilation rates

163 used for standard animal husbandry, intended to prevent excessive humidity and

164 ammonia and CO_2 accumulation, were incompatible with retention of aerosolized

165 particles. Successful transmission would likely require precise titration of airflow to

166 maintain particle dwell time without compromising animal welfare.

167 Guided by these results, we next developed system 2A, in which air movement was

168 driven solely by the exhaust fan (2.5 L/min). This modification improved particle

169 retention within both donor and recipient compartments under ambient conditions,

170 especially for particles less than 2µm (Fig. 2F-G).

171 Inspection of system 1 also revealed a structural limitation: its double-walled stainless-

172 steel barrier created a wide and obstructed path for particle transfer between

173 compartments. To address this, we engineered a new single-walled stainless-steel

174 barrier with larger perforations to reduce physical impedance to airflow. We also sealed

175 the cage to minimize leakage by taping the lid with aluminum tape, adding a rubber

176 gasket along the lid-base junction, and securing the lid with four spring-loaded clamps.

177 The resulting configuration, designated system 2B, was designed to optimize both

airflow continuity and particle containment (Fig. 2H). Under ambient pressure, system

2B achieved particle retention comparable to system 2A, with stable concentrations of

particles <2μm in both compartments (Fig. 2I). The similarity between the two systems

suggested that the improvements achieved by airflow titration and cage sealing were

robust across minor design variations. However, because all prior experiments without

transmission had occurred under negative-pressure BSL-3 conditions, further testing

under those settings was essential to evaluate real-world performance.

Negative pressure and associated airflow profoundly influence particle retention

Because all Mtb transmission studies must be performed under BSL-3 conditions, the

next critical step was to evaluate how negative pressure, an essential safety feature,

affects particle movement within the cage systems. To do this, we placed each system

inside a custom airtight chamber maintained at the negative-pressure setting used in

our ABSL-3 facility (relative negative pressure -0.03 WC) (Fig. 3A). Of note, only system

0 cages were tested at -0.06 WC because the room in which the system 0 cages were

maintained during their use for transmission studies was at -0.06 WC, whereas for

system 1 and 2B, the animal rack was in a room with -0.03 WC relative negative

pressure. Under these conditions, we observed a striking loss of aerosolized particles in

both donor and recipient compartments of system 0 (Fig. 3B, C). The unsealed cage

design allowed particles to escape through lid gaps and barrier edges, resulting in near-

complete depletion of particles across all measured size ranges. System 1 also

exhibited substantial particle loss under negative pressure, particularly in the recipient

compartment (Fig. 3D, E), indicating that unidirectional airflow alone could not

overcome the strong external flow imposed by facility ventilation. System 2A, which

incorporated reduced exhaust flow and a modified barrier, also showed lower particle

retention in the recipient compartment (Fig 3F, G). The most dramatic improvement was

achieved with system 2B, which combined controlled exhaust flow with cage sealing.

Under negative pressure-induced flow, system 2B maintained high concentrations of

aerosols within both donor and recipient compartments, demonstrating markedly

improved particle retention compared to all previous iterations (Fig. 3H, I).

Together, these results reveal that negative pressure-induced flow profoundly alters

internal cage mixing, often removing aerosols before they can traverse from donor to

recipient compartments. Through progressive modification of airflow, barrier design, and

cage sealing, system 2B successfully counteracted these losses, providing stable

particle retention even under the stringent airflow conditions required for BSL-3

containment. This optimized configuration was therefore selected for subsequent

transmission experiments.

Biological factors impacting transmission

We next evaluated the impact of environmental variables on transmission efficiency in

our optimized cage system. To model movement of bacteria-containing particles, we

nebulized a suspension of *Mycobacterium smegmatis,* a non-pathogenic mycobacterial

species, in the donor compartment and measured bacterial recovery from air sampled

on the recipient side. Recovery of *M. smegmatis* showed a clear dependence on airflow

rate, with the highest recovery observed at the lowest exhaust setting of 0.15 L/min (Fig.

4A). This pattern suggested that reduced airflow prolongs particle dwell time within the

cage and enhances the likelihood of bacterial transport between compartments.

We then tested if aerosolized bacteria from the donor compartment could deposit into

the lungs of naïve guinea pigs housed on the recipient side. We placed individual

guinea pigs in the recipient compartment and nebulized a suspension of *M. smegmatis*

in the donor compartment for one minute to simulate a cough paroxysm. After 15

minutes of exposure to *M. smegmatis*, we collected and homogenized the lungs of

recipient guinea pigs and quantified colony forming units (CFU). All four recipient guinea

pigs had recoverable *M. smegmatis* CFU in their lungs (Fig. 4B), demonstrating that

aerosolized bacteria generated in the donor compartment were effectively transported

and inhaled by recipient animals.

Because humidity strongly influences aerosol dynamics by affecting particle desiccation

and settling (Bourouiba, 2021; Li et al., 2021), we next quantified relative humidity (RH)

in occupied cages. We housed two guinea pigs (one per compartment) for six days in

system 2B cages, and measured RH daily at three exhaust flow rates (2.5, 1.5, and

0.15 L/min). At the lowest airflow rate, humidity rose rapidly, reaching approximately 75

percent by day six (Fig. 4C). Higher airflow rates maintained RH near 65% throughout

the experimental, consistent with enhanced air exchange and moisture removal (Fig.

4C). Although lower exhaust flow improved particle transport, the associated increase in

humidity was expected to impair aerosol stability and potentially affect animal welfare

during long term studies. Based on these considerations, we selected an exhaust flow

rate of 2.5 L/min for subsequent Mtb transmission experiments using system 2B.

Mtb transmission under optimized conditions

Having established airflow and environmental parameters that favored particle retention,

we next assessed whether these optimized conditions supported Mtb transmission

between guinea pigs. We infected guinea pigs with Mtb (Suppl. Fig 2A) and placed

them in the donor compartment of system 2B cages, while naïve guinea pigs were

housed in the recipient compartment for a 17-week exposure period. Because guinea

pigs develop progressive disease following infection, donor animals were replaced

every six weeks to maintain a consistent infectious source.

We monitored for transmission with monthly TST analysis using a two-stage protocol

(2000; Jensen et al., 2005; Taylor et al., 2005) by testing animals twice with a 7-day

waiting period between doses (Fig. 5A). We also performed TSTs on all donor animals

after 4 weeks of infection. Donor animals developed robust TST responses (mean 10

mm; range 6-16 mm), consistent with active infection (Fig. 5B). To define a threshold for

positive conversion in recipients, we performed repeated TSTs in unexposed control

animals and found that none exceeded 5.5 mm. Using this as a baseline, combined with

TST data from Mtb-infected donor animals and uninfected naïve animals, we

established a TST cutoff of 6.5 mm to indicate infection (Suppl. Fig 2D-E). Within one

month of exposure, one recipient exceeded this threshold, and by week 17, nine of

twelve recipient animals demonstrated positive TSTs (Fig. 5B, Suppl. Fig 3).

While TST is a measure of cell-mediated immunity, Mtb exposed individuals also

develop humoral responses indicative of exposure or infection (Davies et al., 2023;

Davies et al., 2024; Kroon et al., 2020; Lu et al., 2016; Lu et al., 2020; Lu et al., 2019).

Thus, to corroborate the TST results with an independent immunologic measure, we

quantified serum antibody responses to Mtb antigens representing either complex

mixtures (such as PPD) or defined highly immunogenic proteins such as antigen 85B

using a bead-based multiplex assay (Suppl. Fig. 4A) (Lu et al., 2019). We calculated the

AUC (area under the curve) for each antigen using a dilution curve and generated ROC

(receiver operating characteristic) curves for individual or combination antigen-specific

IgGs (Suppl. Fig. 4B-G). Infected donors exhibited strong IgG responses to both

antigens, whereas unexposed controls remained negative. Using an ROC predictive

probability cutoff of 0.5 for the combined IgG response to antigen 85B and PPD (Suppl.

Fig. 4H), eight of twelve recipient animals displayed serologic responses consistent with

Mtb exposure (Fig. 5C).

We next examined lung tissues from recipient guinea pigs by blinded histopathology

analysis. Compared to unexposed controls, exposed recipients exhibited increased

pulmonary inflammation characterized by stage 1 granulomas, intra-alveolar

hemorrhage, and small foci of epithelioid macrophages (Fig. 6D-E, Suppl. Fig. 2F-G).

Although no culturable Mtb was recovered, the combination of TST conversion,

serologic response, and histopathologic evidence indicated that recipient animals had

been exposed to and immunologically responded to Mtb.

Together, these results demonstrate that the optimized system 2B configuration

supports natural transmission of Mtb between infected and naïve guinea pigs. The

integration of controlled airflow, cage sealing, and structural refinement enabled

sufficient aerosol retention to permit infection under BSL-3 containment, providing a

reproducible experimental model for studying the determinants of airborne TB spread.

DISCUSSION

Our current understanding of TB transmission arises largely from epidemiologic studies

of Mtb spread within human populations or from analysis of exhaled aerosols (Fennelly,

2020; Fennelly et al., 2012; Fennelly et al., 2004; Lan et al., 2025; Patterson et al.,

2025; Tristao et al., 2025). Experimental validation of these observations has been

constrained by the lack of modern animal-to-animal transmission systems. Using a

multidisciplinary approach that integrates flow physics, engineering, and infection

biology, we developed an optimized guinea pig model that captures the essential

features of natural Mtb transmission. This system preserves airborne infectious particles

expelled by donor animals and facilitates their transfer to susceptible recipients, thereby

enabling mechanistic studies of transmission.

Through iterative optimization, we identified airflow as a key determinant of

transmission. Retention of particles within the 1-5 μm range, which can carry Mtb

(Fennelly, 2020; Fennelly et al., 2012; Fennelly et al., 2004; Tristao et al., 2025),

required balance between airflow rate and containment parameters. Static

environments lost particles to the environment and limited aerosol transport, while

excessive ventilation air changes eliminated particles before they reached the recipient

compartment. By defining the airflow range that allows aerosol particle persistence, we

successfully achieved transmission under negative-pressure BSL-3 conditions.

Recipient animals mounted measurable immune responses to Mtb antigens and

displayed pulmonary inflammation consistent with early infection. These results

demonstrate that natural airborne transmission of Mtb can be reconstituted when airflow

is tailored to favor airborne particle retention and exposure.

The influence of overall ventilation on infection risk has long been recognized, from the

classic studies of Riley and Wells, to modern public health strategies for airborne

disease control. The COVID-19 pandemic renewed attention to air exchange rates as a

means of mitigating transmission in hospitals and community settings (Bourouiba,

2020). However, such ventilation strategies pose challenges when modeling infectious

disease transmission experimentally. Our results show that both overly static and overly

ventilated systems suppress transmission, providing a biophysical explanation for the

scarcity of animal-to-animal models since the advent of modern biosafety facilities. In

addition, our results provide experimental confirmation that airborne TB transmission

can be mitigated with sufficient replenishment of fresh air (Beggs et al., 2003; Escombe

et al., 2007b; Granich et al., 1999; Jensen et al., 2005; W.H.O., 2024), as illustrated by

our experimental outcomes showing absence of animal-to-animal transmission in

systems 0 and 1. By accounting for these aerodynamic constraints, our study

establishes a framework for designing experimental systems that control airflow

intensity and patterns and can faithfully model airborne pathogen spread under safe

laboratory conditions.

The ability to reproduce natural transmission has important implications for

tuberculosis biology. Few tools currently exist to test hypotheses about how bacterial,

host, and environmental factors interact to shape the transmission cascade. Most

experimental systems rely on artificial aerosolization of Mtb to naïve animals (Nuritdinov

et al., 2025), human-to-guinea pig exposure systems (Dharmadhikari et al., 2011;

Escombe et al., 2007a), or small animal models with unknown correlates to human TB

(Gupta et al., 2022; Ramos et al., 2017). The system described here provides a means

to investigate transmission directly between infected and naïve animals in a well-

characterized model of TB disease. It can be adapted to test how microbial factors such

as strain lineage (Coscolla and Gagneux, 2014; Cui et al., 2019; Holt et al., 2018;

Huang et al., 2020; Koleske et al., 2025; Niemann et al., 2010; Yang et al., 2012), lipid

composition (Moopanar and Mvubu, 2020; Naqvi et al., 2025; Ruhl et al., 2020), genetic

background (Verma et al., 2019) or specific Mtb genes (Mishra et al., 2025) affect

transmissibility, and to examine how donor physiology influences aerosol generation

and infection probability.

The relationship between respiratory behavior and transmission remains a particularly

important question. Recent studies have shown that tidal breathing alone can generate

infectious bioaerosols (Dinkele et al., 2022; Dinkele et al., 2024a; Dinkele et al., 2024b),

raising debate about the relative contribution of cough to new infections (Patterson and

Wood, 2019). Coughing, however, produces more particles than quiet breathing and

propels them over longer distances (Bourouiba, 2020; Bourouiba, 2021; Bourouiba et

al., 2014; Li et al., 2021; Tristao et al., 2025; Wang et al., 2025). Our prior work

identified specific Mtb cell wall glycolipids, sulfolipid-1 and phenolic glycolipid, as

sufficient to induce cough in naïve guinea pigs (Naqvi et al., 2025; Ruhl et al., 2020),

and guinea pigs infected with Mtb strains lacking both lipids did not cough, despite

extensive pulmonary pathology (Ruhl et al., 2020). In the context of the current model,

comparing donors that do or do not express these lipids will allow direct testing of how

pathogen-encoded factors that trigger cough influence transmission efficiency.

This study has several limitations. Although recipient animals showed consistent

immunologic and histologic evidence of exposure, we did not recover culturable Mtb

from their lungs. Earlier studies of human-to-guinea pig transmission reported similar

findings, and subsequent immunosuppression with dexamethasone revealed latent

infection (Dharmadhikari et al., 2011). Extending exposure duration or introducing a

recovery phase with transient immunosuppression may increase bacterial detection in

future experiments. Additionally, replacement of moribund donor animals prevented

correlation of donor bacterial burden or cough frequency with recipient infection

outcomes. Future studies will pair physiologic monitoring of donors with environmental

sampling to define the quantitative relationship between aerosol production, bacterial

load, and transmission success.

In summary, this work revives a classical model of airborne tuberculosis transmission

and adapts it for modern biosafety conditions. Through iterative optimization of cage

design and airflow parameters, we demonstrate that airflow governs the transport and

retention of infectious particles and determine the likelihood of transmission. This

system establishes a reproducible physics-informed platform to investigate the

environmental, microbial, and host factors that drive airborne spread of Mtb and to

develop novel pharmacological and non-pharmacological transmission blocking

interventions.

MATERIALS AND METHODS

Animal studies

Protocols for guinea pig infection and transmission studies were reviewed and approved

by the Institutional Animal Care and Use Committee at the University of Texas

Southwestern Medical Center (Protocol # 2018-102280-USDA).

Particle transmission

Aerosol particles were generated using a custom-built particle generation system. A

syringe pump (Braintree Scientific, MA, USA) delivered EMEM (Suppl. fig 1B)

suspension solution at a flow rate of 0.4 mL/min. Compressed air at 60 psi atomized

and dried the aerosols, with a total flow of 21.5 L/min. Relative humidity along the tubing

was monitored with a probe (Ahlborn, Germany) and maintained at 48 ± 2%.

Continuous aerosol loading into the cage was controlled at 0.3 L/min, while excess flow

was vented using a vacuum pump (Gast Manufacturing, MI, USA) regulated by a mass

flow controller (MFC; Aalborg Instruments and Controls, NY, USA).

Four case systems were evaluated: System 0, System 1, System 2A, and System 2B.

Each consisted of donor and recipient compartments separated by a divider, with 0.3

L/min entering the donor side. Flow conditions varied among tests as summarized in

Table 1. Compressed supply air (8.8 L/min) could be directed into the donor side, and

exhaust air (2.5 L/min) was regulated using a custom-built laminar flow element

connected to the facility vacuum.

Table 1: Flow conditions for cage systems

Testing case	System 0	System 1	System 2A	System 2B
Divider Modification	Plexiglass, double wall	Stainless steel, double wall	Stainless steel, double wall	Stainless steel, single wall
Lid sealing	Off	Off	Off	On
8.8 L/min supply	Off	On	Off	Off
2.5 L/min exhaust	Off	On	On	On

Aerosol particle size distributions were measured on both donor and recipient sides

using an Aerodynamic Particle Sizer (APS; Model 3321, TSI, MN, USA). The APS drew

0.3 L/min directly from each sampling site, while dilution air was added through

compressed air controlled by a MFC to achieve the required 5 L/min sampling flow.

Before aerosol introduction, clean air was flushed through the cage for 30 min to

confirm negligible background particle concentrations. Aerosol particles were then

loaded for approximately 1 h to reach steady-state size distributions (Suppl. Fig. 1A).

After loading, three 20-second samples were collected per minute, alternating between

donor and recipient sides. The particle size boundary was set to 0.8-7µm. Sampling was

repeated every 5 min over a 25-min period under both ambient and negative-pressure

conditions.

To reproduce biosafety level 3 negative-pressure environments, a custom chamber (24″

× 24″ × 48″) was constructed. An inline duct fan (TerraBloom LLC, CA, USA) regulated

airflow, and chamber pressure was monitored continuously using a differential gauge

(Dwyer Instruments, Inc., IN, USA), maintained at –0.03 inches of water.

Mycobacterium smegmatis particle transmission

Mycobacterium smegmatis cultures were grown in Middlebrook 7H9 broth (Sigma

#M0178) supplemented with 10% OADC, 0.5% glycerol, and 0.05% Tween-80 at 37 °C

with shaking (100 rpm). Cultures were diluted to $1 \times 10\square$ CFU/mL in PBS and

aerosolized using a Blaustein Atomizing Module (CH Technologies). The atomizer was

placed in the donor compartment of the transmission cage, and aerosols were

generated for 1 min. After a 2-min delay, air from the recipient compartment was

sampled for 30 s using a button sampler (SKC, PA, USA) with a gelatin filter at 10 L/min.

The filter was dissolved in PBS and plated on Middlebrook 7H10 agar supplemented

with OADC and glycerol. Colonies were counted after overnight incubation to quantify

recovered bacteria. This procedure was repeated at exhaust flow rates of 2.5, 1.5, and

0.15 L/min.

For transmission of *M. smegmatis* to guinea pigs, the atomizer was placed in the donor

compartment containing 1×10^5 CFU/mL of *M. smegmatis* in PBS. The recipient

compartment contained 2 guinea pigs. Aerosols were generated for 1 min and allowed

to pass to the recipient compartment and inhaled by the recipient animals for 15

minutes. Following the 15-minute period, animals were sacrificed and lungs were

homogenized in PBS and plated on four 7H10 agar plates per animal to quantify

recovered bacteria. This process was repeated for a total of four guinea pigs.

Guinea pig aerosol infection

Donor guinea pigs were infected with *M. tuberculosis* Erdman in three groups on a 6-7

week cycle. Bacteria were cultured in Middlebrook 7H9 broth supplemented with 10%

OADC, 0.5% glycerol, and 0.05% Tween-80 at 37 °C using a roller apparatus. Cultures

were washed three times with PBS and resuspended, then centrifuged at 500 rpm for 5

min to remove large clumps. The supernatant was sonicated at 90% amplitude for 15-s

pulses (Branson Ultrasonics, CT, USA) to generate a single-cell suspension and diluted

to $3 \times 10\square$ CFU/mL. The inoculum was aerosolized using a Glas-Col inhalation

exposure system (Glas-Col, IN, USA). Two animals per group were sacrificed

immediately post-exposure for day-0 CFU quantification by lung plating on 7H11 agar.

All animals were weighed weekly, and donors were euthanized seven weeks post-

infection.

Transmission experiments and cage modifications

For transmission experiments, male Hartley guinea pigs (Charles River) were used. For

system 0, we used a polycarbonate static cage (Tecniplast # 2000P00SU), with a raised

lid (Tecniplast #2000P224) covered by a filter top (Tecniplast #2000P400SU) that used

conventional static cage top filters (Tecniplast #U1144B420RBOX-300) with a custom

designed double walled plexiglass divider perforated with holes for particle movement

between compartments. For the transmission experiment, cages were maintained on a

stainless-steel rack in our ABSL3. For systems 1 and 2B, we housed animals in an

Allentown 1800 15 cage rack (Allentown, NJ, PA). The standard cage bottom (Allentown

#315351-1) and external bottle top (Allentown #230347) were used with the following

modifications. For both system 1 and 2B, the donor-side exhaust port (right) and

recipient-side supply ports (left) were sealed with rubber caps. While for system 1 the

supply air was "on", for system 2B, the supply hose was disconnected from the main air

inlet of the rack. For system 2B, a custom stainless-steel cage divider with 102

ventilation holes was fabricated locally to separate donor and recipient animals within

each cage. To improve sealing, the underside of the lid was covered with aluminum

tape, a 1.6 mm rubber gasket was applied along the lid-base junction, and four 2-inch

spring clamps secured the lid once cages were positioned on the rack.

Tuberculin skin test

To determine Mtb exposure, guinea pigs were tested every four weeks using a two-step

TST protocol. Animals were anesthetized under 3% isoflurane, and the right or left flank

was shaved and cleaned with 70% ethanol. Tuberculin purified protein derivative (PPD;

100 µL of 5 TU, McGuff Medical Products #001079) was injected intradermally.

Induration was measured at 24 h and 48 h post-injection. The procedure was repeated

one week later on the opposite flank. Control animals received a single dose of

tuberculin at baseline or the same number of total doses (seven) as exposed animals to

control for effects of repeated testing.

Serologic analysis

Antigen-specific IgG levels were quantified as previously described with minor

modifications (Adhikari et al., 2024; Bates et al., 2022; Lu et al., 2019). Carboxylated

microsphere beads (Luminex Corp., Austin, TX, USA) were coupled to protein antigens

via covalent NHS-ester linkages using 1-ethyl-3-[3-dimethylaminopropyl] carbodiimide

hydrochloride (EDC) and *N*-hydroxysulfosuccinimide (NHS) (Thermo Fisher Scientific,

Waltham, MA, USA), following the manufacturer's instructions. MagPlex® Avidin

microspheres (Luminex) were conjugated to biotinylated sulfolipid-1 (SL-1) using the

manufacturer's protocol.

The following antigens were used: Ag85A (BEI Resources NR-14871), Ag85B (NR-

14870), ESAT-6 (NR-49424), CFP-10 (NR-49425), purified protein derivative (PPD;

Statens Serum Institute, Copenhagen, Denmark), *M. tuberculosis* H37Rv whole-cell

lysate (NR-14822), and *M. tuberculosis* H37Rv cell wall fraction (NR-14828).

Antigen-coupled microspheres (1,000 beads per well) were incubated with diluted

guinea pig serum (1:50, 1:250, and 1:1,250) in 96-well Bio-Plex Pro flat-bottom plates

(Bio-Rad Laboratories, Hercules, CA, USA) at 4 °C for 16 h. After washing to remove

unbound antibodies, antigen-specific IgG was detected using phycoerythrin (PE)-

conjugated goat anti-guinea pig IgG (Novus Biologicals, NBP1-74874PE). Beads were

incubated with the secondary antibody for 2 h at room temperature, washed with PBS

containing 0.05% Tween-20, and resuspended in PBS. Fluorescence intensity was

acquired using a MAGPIX® instrument running xPONENT 4.2 software (Luminex).

Relative antigen-specific IgG levels were quantified as the area under the curve (AUC)

calculated from the three serial serum dilutions for each sample.

Receiver operating characteristic (ROC) curves were generated using GraphPad Prism

version 10.5 (GraphPad Software, San Diego, CA, USA). Sensitivity and specificity at

selected cutoff points, along with 95% confidence intervals, were calculated using

logistic regression.

Histologic analysis

At study completion, animals were euthanized, and lungs were collected in 10% neutral-

buffered formalin for histopathologic analysis. Fixed tissues were transferred to 70%

ethanol and processed by the Histo Pathology Core Facility at UT Southwestern.

Paraffin-embedded blocks were sectioned at 5 µm and stained with hematoxylin and

eosin. Slides were scanned using a NanoZoomer S60 digital slide scanner, randomized,

and blinded prior to evaluation by a pathologist. The number and stage of granulomas

were recorded, and pulmonary inflammation was described for each animal. After

unblinding, data were compared between naïve and exposed animals using a Mann-

Whitney test (GraphPad Prism v10).

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DECLARATION OF COMPETING INTERESTS

All authors declare that they have no competing interests.

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 Figure legends

Figure 1: Airflow Modifications of Preliminary Transmission Systems (A) Experimental

scheme for 12-month transmission studies. Blue ticks indicate when new donor groups

were added to cages and stars denote when TSTs were performed. (B) System 0 cage

set up with static airflow and plexiglass divider between donor and recipient

compartments. (C) 15 cage rack as available by Allentown, Inc. (D) System 1 cage set

up. Donor side is connected to supply hose which delivers 8.8 LPM into the cage. Air

then passes through a stainless-steel divider to recipient compartment and is exhausted

at 2.5 LPM. (E) Modifications to cage rack include plugging the exhaust port on the

donor side and supply port on the recipient side to drive unidirectional airflow. (F)

Smoke test to confirm unidirectional movement of air within system 1. See also

supplemental movie 1.

Figure 2: Particle movement driven by airflow under ambient pressure. (A) Experimental

overview of particle transport. Cage systems are connected to supply air (where

applicable) and exhaust vacuum to control airflow within the cages. Particles are

introduced to the donor compartment using a particle generator. An APS particle

sampler collects particles upstream before entering the cage, in the donor and recipient

compartments. (B-C) Schematic and particle sampling of System 0 under static flow

conditions. (D-E) Schematic and particle sampling of System 1 with supply air set to 8.8

LPM and exhaust to 2.5 LPM. Dashed line indicates unsealed cage lid. (F) System 2A

schematic with air supply removed (0LPM) and exhaust set to 2.5 LPM. (G) Particle

transport within system 2A. (H-I) Schematic and particle transport of system 2B

modified to include cage lid sealing (solid line) and a single stainless-steel barrier. All

particle transport results are represented as number of particles per cubic centimeter of

air (#/cc) in the size range of 0.8-7 µm. Sampling of particles includes upstream (red)

before entering the cage, in the donor compartment (blue) and the recipient

compartment (black).

Figure 3: Negative pressure influences retention of particles within cage systems. (A)

Experimental set-up of particle transport where cage systems are placed inside a

custom chamber under negative pressure (-0.03 WC). (B-C) System 0 cage design and

particle movement within cage system while under negative pressure. (D-E) Addition of

unidirectional airflow in system 1 design and particle transport within system 1. Dashed

line indicates unsealed cage lid. (F-G) Schematic of system 2A with airflow driven by the

exhaust port (2.5LPM) and particle transport under negative pressure conditions. (H-I)

System 2B schematic with modified cage lid sealing (solid line) and single cage barrier

and particle transport within system 2B. All particle transport results are represented as

number of particles per cubic centimeter of air (#/cc) in the size range of 0.8-7 µm.

Sampling includes upstream (red) before entering the cage, in the donor compartment

(blue) and the recipient compartment (black).

Figure 4: Optimization of biological factors which influence transmission efficiency. (A)

Recovery of particles containing *M. smegmatis* from the recipient compartment using a

low-flow button sampler at varying exhaust flow rates (0.15, 1.5 and 2.5 L/min). (B)

Nebulization of *M. smegmatis* in the donor compartment and recovery of bacteria from

lungs of recipient guinea pigs in system 2B cages. Colony forming units (CFU)

quantified from lung homogenates plated across four agar plates from four different

guinea pigs. Each point represents CFU on an individual plate. (C) Humidity

accumulation during guinea pig housing in system 2B cages. Relative humidity (%) in

three system 2B cages with guinea pigs housed in each compartment (two per cage)

across 6 days. Three different exhaust flowrates tested include 0.15, 1.5, and 2.5 L/min.

Cages were changed at day 4 for all flowrates.

Figure 5: Transmission of Mtb in an optimized cage system. (A) Experimental timeline

for 17-week transmission study. Blue ticks indicate when new donor groups were added

to the cages. Monthly TSTs using a prime/boost strategy are noted as filled stars (prime

dose) and open stars (boost dose). (B) TST measurements for recipient animals

throughout the exposure period. Any responses above 6.5 (dashed line) are considered

positive. (C) Predicted probability of Mtb exposure based on serum antigen 85B and

PPD IgG levels. Values above 0.5 (dashed line) are predicted positive in the donor,

naïve, recipient and TST control groups. (D) Quantification of stage 1 granulomata in

naïve and recipient lung sections. (E) Representative hematoxylin and eosin staining of

lung section from naïve and recipient groups. Inflammatory collection (naïve) and stage

1 granuloma (recipient) at 20x. p-values calculated by one-way ANOVA for multiple

comparisons or Mann-Whitney for comparison between two groups. ns=not significant,

*=p<0.05, **= p<0.01, ***=p<0.001, ****=p<0.0001.

Supplemental Figure 1: Particle generation within cage systems. (A) Concentration

equilibrium within cage systems from 6 to 84 minutes of continuous generation. (B)

chemical composition of EMEM used for particle generation.

Supplemental Figure 2: Animal characteristics of transmission study (A) Lung CFU

directly after aerosol infection (day 0) for donor groups 1,2, and 3. (B) Weight tracking of

donor guinea pigs over 7 weeks (group 1 and 2) and 5 weeks for group 3. (C) Weight

tracking of recipient guinea pigs throughout 17-week exposure period. (D) TST

measurement in TST control guinea pigs given 7 doses of tuberculin. (E) TST

measurement in naïve guinea pigs given one prime and boost dose of tuberculin.

Dashed line denotes cut-off (6.5 mm) for positive responses. (F) Hematoxylin and eosin

staining of lung sections from 8 naïve animals used for histopathology analysis. (G)

Lung sections from 12 recipient animals stained with hematoxylin and eosin for

histology analysis.

Supplemental Figure 3: TST measurements of individual recipient guinea pigs. TST

measurements for each recipient guinea pig (#1-12) across the exposure period. Any

values above 6.5 mm (dashed line) are considered positive. Recordings include the

prime and boost dose of tuberculin.

Supplemental Figure 4: Serum antibody levels of guinea pigs. (A) experimental design

of bead-based serum antibody quantification. (B) Area under the curve (AUC) of SL-1

specific IgG for donor, naïve, recipient, and TST control groups. Receiver operation

characteristic (ROC) curve predictive power (%) for both positive and negative values

based on SL-1 antigen specific IgG. (C-G) AUC and ROC curves for cell wall, whole cell

lysate, ESAT6 CFP10, PPD, and Antigen 85B specific IgG. (H) ROC curve for combined

antigen 85B and PPD IgG.

Figure 1

Figure 2

A

Exhaust vacuum

Room Pressure

System 0-2B

Supply air

Recipient

Donor

APS Particle sampler

Particle generator

B System 0

C

D System 1

Exhaust 2.5LPM

Supply 8.8 LPM

E

F System 2A

Exhaust 2.5LPM

Supply 0 LPM

G

H System 2B

Exhaust 2.5LPM

Supply 0 LPM

I

Legend (C, E, G, I): Upstream, Donor, Recipient

Axes: Particles counted #/cc vs Particle size (µm)

Figure 3

A

Exhaust vacuum

Negative Pressure

Supply air

System 1-2B

Recipient   Donor

Particle generator

APS Particle sampler

B   System 0

C
Particles counted #/cc
- Upstream
- Donor
- Recipient
Particle size (µm)

D   System 1

Exhaust 2.5LPM   Supply 8.8 LPM

E
Particles counted #/cc
- Upstream
- Donor
- Recipient
Particle size (µm)

F   System 2A

Exhaust 2.5LPM   Supply 0 LPM

G
Particles counted #/cc
- Upstream
- Donor
- Recipient
Particle size (µm)

H   System 2B

Exhaust 2.5LPM   Supply 0 LPM

I
Particles counted #/cc
- Upstream
- Donor
- Recipient
Particle size (µm)

Figure 4

Figure 5