An atlas of microtubule lattice parameters regulated through ligand
binding to the microtubule stabilizing sites.

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ABSTRACT

Microtubules (MTs) are essential cytoskeletal polymers with dual functions: they generate

mechanical forces necessary for processes such as mitosis and angiogenesis, and serve as static

tracks for intracellular transport by motor proteins. Force generation is mediated by the cytomotive

switch, a dynamic property modulated by MT stability. Second-generation microtubule-targeting

agents (MTAs), such as paclitaxel and docetaxel, bind at the taxane site and chemically stabilize

MTs by enhancing lateral and longitudinal tubulin interactions. While effective in blocking MT

depolymerization and preserving transport, the fact that these drugs introduce structural

alterations that distinguish stabilized MTs from their native counterparts raises concerns for both

mechanistic studies and clinical applications in diseases like tauopathies.

In this study, we provide a detailed structural atlas of taxane site-mediated modulation of

MTs. We show that drug binding induces two distinct lattice conformations in the longitudinal

axis—expanded (4.17 nm rise) and compressed (4.06 nm rise)—with rapid transitions and low

energy barriers between them. In contrast, lateral interactions allow multiple protofilament (PF)

configurations with small energetic differences but high activation barriers, a finding consistent

with the observed structural heterogeneity of MTs. Notably, minor chemical modifications, such

as acetylation of paclitaxel's C-7 hydroxyl, can shift these conformational equilibria. These

structural changes significantly impact biochemical properties, and alter recognition by tau and

kinesin proteins, suggesting a role for lattice conformation as a signaling cue. Our findings

underscore the nuanced structural consequences of taxane-site ligand binding and its relevance

in both therapeutic and experimental contexts.

Introduction

Microtubules (MTs) are cellular structures involved in many essential biological processes. They are polymers composed of tubulin, a heterodimer of α- and β-tubulin, which serves as their main structural component. Microtubules are responsible for generating cellular forces, maintaining cell shape, and providing polarized tracks for directional, motor-mediated chemical transport [1].

Tubulin, together with actin, generates mechanical forces by coupling nucleotide hydrolysis to its polymerization cycle. Both proteins undergo assembly state-dependent conformational changes that are intrinsically linked to their ability to produce force—a mechanism known as the cytomotive switch [2]. In tubulin, this switch entails a curved-to-straight conformational transition characterized by an interdomain rotation between the N- and C-terminal domains of each monomer, accompanied by a downward displacement of helix H7 [3-5].

Because this conformational change is essential for force generation, compounds that block the transition inhibit cellular processes that depend on mechanical force—such as cell division and angiogenesis—thereby severely compromising cell function. Consequently, many sessile organisms have evolved to produce tubulin-targeting anticytomotive compounds as a defense mechanism against predators [6]. These compounds bind to the αβ-tubulin heterodimer on at least eight distinct binding sites [7-9], employing four main mechanisms to block the cytomotive switch.

Compounds that inhibit MT formation act on six distinct binding sites—those of colchicine, vinblastine, maytansine, pironetin, gatorbulin, and todalam. These compounds block the cytomotive switch through two main mechanisms:

(i) some compounds bind at the intradimer interface, acting as molecular wedges that trap tubulin in the assembly-incompetent curved conformation. Representative examples include colchicine, derived from *Colchicum autumnale*, the extract from which as a gout treatment has been documented since 1500 BC [10]; mebendazole, a well-established anthelmintic [11]; and gatorbulin, a recently discovered tubulin inhibitor that binds to a novel site[8].

(ii) other compounds that block longitudinal interdimer interfaces, such as vinblastine, the first tubulin-targeting agent approved for cancer therapy [12]; maytansine, one of the most widely used payloads in antibody-drug conjugates (ADCs) [13], and pironetin [14]. By binding at these longitudinal contacts, these ligands prevent the addition of new subunits and subsequently the conformational transition [15-18]. As a result, ligand-bound subunits become inactive, leading to the collapse of the microtubule network and inhibition of cell division in rapidly proliferating cells, such as leukemic cells.

Although first-generation tubulin inhibitors (e.g., vinca alkaloids) are highly effective against rapidly dividing tumors—by blocking the force generation required for cell division and migration—their mechanism of action involves the destruction of microtubules. These compounds inhibit the cytomotive switch in the curved-to-straight direction, thereby preventing polymerization. Consequently, they indiscriminately block all tubulin-mediated functions, not only those related to force generation but also structural roles essential for intracellular transport, axonal integrity, and

neural transmission. This broad inhibition leads to one of the most limiting side effects in
successful cancer therapy: peripheral neurotoxicity, caused by damage or degeneration of
peripheral nerves (19).

Paclitaxel (Taxol®) was the first representative of the second generation of microtubule-
targeting agents (MTAs), approved for clinical use in 1992 (20). This second family, later
expanded to include docetaxel (Taxotere®), cabazitaxel (Jevtana®), and ixabepilone (Ixempra®),
acts through the opposite mechanism to that of the vinca alkaloids—blocking the cytomotive
switch in the straight-to-curved direction. The resulting stabilization of microtubules defines these
compounds as microtubule-stabilizing agents (MSAs).

Structural studies of MSA–tubulin interactions have revealed two distinct mechanisms,
involving two different binding sites, that prevent the straight-to-curved transition. Most known
MSAs—including taxanes, epothilones, discodermolides, and zampanolides—bind to the taxane
site, where they reinforce lateral contacts between tubulin subunits by pushing the S9–S10 loop
(M-loop) toward the interprotofilament (IPF) space (21). In contrast, compounds that bind to the
laulimalide/peloruside site (22) stabilize MTs by bridging adjacent PFs, thereby also preventing
the straight-to-curved transition. Although this mechanism should, in principle, selectively target
MT force-generating functions while preserving their structural and trafficking roles, MSAs exhibit
peripheral neurotoxic effects that are comparable to—or even more severe than—those caused
by microtubule-destabilizing agents (MDAs) (23, 24).

Structural studies on the most commonly used second-generation microtubule-targeting
drugs indicate that their stabilizing effect on microtubules is not without structural consequences.
Binding of paclitaxel and docetaxel to the taxane site induces a longitudinal expansion of the
microtubule lattice, increasing the dimer repeat distance from 4.06 nm to 4.17 nm; in the case of
paclitaxel, this also enlarges the IPF angle, resulting in thinner MTs (21). In contrast, compounds
that bind to the laulimalide/peloruside site stabilize MTs without lattice expansion, although they
cause distortions at the lateral interface. Nevertheless, it is possible to design compounds
targeting this site—such as pelophen B—that stabilize MTs without introducing structural
distortions (25).

MT structure plays a central role in its own regulation, which occurs at several levels, the
first being the nucleotide bound to the exchangeable site. Tubulin bound to GTP incorporates into
the growing plus end of the MT. Because the nucleotide binding site lacks a catalytic residue
required for hydrolysis—supplied instead by the next incoming tubulin subunit—activation of
GTPase activity occurs stochastically. As a result, a chemical gradient is established along the
MT, from GTP-bound tubulin at the plus end to GDP-bound tubulin within the lattice core. In this
way, the nucleotide-driven chemical gradient is translated into subtle structural variations within
the MT lattice that are recognized by microtubule-associated proteins (MAPs) (1, 26). MAPs
represent the principal endogenous regulators of MT dynamics and orchestrate the structural
remodeling of MT networks, which is essential for optimal cellular functionality (27). Several
examples illustrate this structural recognition. End-binding (EB) proteins display selective affinity
for the GTP-rich plus ends of microtubules (28), while tau and kinesin exhibit preferential binding

to lattices with specific monomer-to-monomer spacings. Kinesin-1, for instance, shows enhanced affinity in gliding assays for MTs with an expanded lattice (4.17 nm spacing) (29), whereas tau preferentially associates with compacted lattices (4.06 nm spacing).

Moreover, *in vitro* evidence demonstrates that tau cooperatively induces lattice compaction in microtubules that have been exogenously expanded by paclitaxel (30), whereas kinesin has been shown to promote lattice expansion (31). These differential preferences likely reflect the dual functional capacity of these proteins to both recognize specific conformational states and actively remodel the microtubule lattice. Collectively, the literature suggests that tau and kinesin act as both sensors and effectors of the MT lattice. Consequently, compounds that induce structural distortions in MTs are expected to strongly influence MAP recognition and activity, thereby disrupting the regulation of MT dynamics and function (32).

Given the central role of tubulin-targeted therapies and their potential to address inflammatory, neoplastic, and neurodegenerative diseases, it is of utmost importance to understand how MSAs alter MT structure. To shed light on the structural signals that arise within the microtubular lattice and their relevance for MAP recruitment, we have compiled this atlas. In this work, we characterize the structural effects induced by different chemotypes from the two major families of MSAs using fiber diffraction analyses of aligned MTs and computer simulations. In parallel, through TIRFM (Total Internal Reflection Fluorescence Microscopy)-based assays, we examine how these structural alterations influence the interaction of two key MAPs, tau and kinesin, with the modified filaments. This integrated knowledge provides the microtubule community with the tools to chemically manipulate MT structure at will, offering new opportunities to unravel the principles governing MT regulation and to design safer and more potent tubulin-targeting agents.

Results.

Fiber diffraction analysis of chemically stabilized microtubules.

Previous studies from our group demonstrated the strong influence of paclitaxel (21, 33, 34) and other taxanes (21, 35, 36) on MT structure, inducing both alterations in the number of PFs of the polymer and, as a common feature, an expansion of the MT lattice reflecting a change in the helical pitch from 4.06 nm to 4.17 nm. Such an expansion has been previously observed in hyper-stabilized MTs assembled in the presence of the slowly hydrolysable nucleotide analog GMPCPP (37-39) as well as in catalytically inactive αE254A and αE254N MTs (40). This finding led to the hypothesis that expansion was linked to the activated state of tubulin despite the fact that both GMPPCP and metal fluoride (BeF_3^- and AlF_4^-) stabilized MTs in the compressed state (34). Moreover, doubly activated paclitaxel- and BeF_3^--bound MTs are also in the compressed state (34) and this expansion can be induced by the otherwise biochemically and cellular inactive baccatin III (a precursor of paclitaxel biosynthesis lacking the C-13 side chain) (21). This suggests that the observed lack of compression in GMPCPP and in the catalytically inactive MTs is due to the inability of the catalytic residue Gluα254 to interact with the γ-phosphate,

Figure 1. Chemical structures of the MSAs employed in the study.

either because of the geometric restraints imposed by GMPCPP or as a result of the amino acid replacement.

In order to understand the molecular mechanisms that determine the structural regulation of MTs by chemicals able to stabilize them we employed fiber diffraction of aligned MT samples (41) to determine their structural parameters (**Table I**) in the presence of a library of MSAs (**Figure 1**) covering a variety of chemotypes of both taxane and peloruside/laulimalide sites, including taxanes, epothilones, discodermolide, zampanolides, taccalonolide, cyclostreptin, as well as different perolusides (including synthetic analogs) and laulimalide. Those conditions already published by our group (21, 25, 34, 42) were re-measured and/or re-analyzed to ensure an exact comparison between all figures presented.

Drug	J_{02}[1]	Radius[2]	Avg PF num[3]	1 nm^{-1} band	Avg monomer rise	State[4]
Non drug-stabilized MTs						
Apo	0.0892 ± 0.0001	11.72 ± 0.01	12.91 ± 0.02	0.987 ± 0.001	4.05 ± 0.01	C
GMPCPP	0.0883 ± 0.0003	11.83 ± 0.04	13.05 ± 0.04	0.960 ± 0.001	4.17 ± 0.01	E
GDP·BeF$_3^-$	0.0935 ± 0.0001	11.18 ± 0.01	12.32 ± 0.01	0.979 ± 0.007	4.08 ± 0.03	C
GDP·AlF$_4^-$	0.0908 ± 0.0005	11.51 ± 0.06	12.69 ± 0.07	0.986 ± 0.001	4.05 ± 0.03	C
Taxanes						
PTX	0.0937 ± 0.0002	11.15 ± 0.03	12.29 ± 0.03	0.958 ± 0.001	4.17 ± 0.02	E
PTX+CPP	0.0918 ± 0.0004	11.38 ± 0.05	12.54 ± 0.05	0.955± 0.003	4.18 ± 0.02	E
PTX+BeF$_3^-$	0.0923 ± 0.0001	11.32 ± 0.01	12.48 ± 0.05	0.994± 0.003	4.03 ± 0.03	C
PTX+AlF$_4^-$	0.0918 ± 0.0002	11.38 ± 0.01	12.55 ± 0.03	0.991± 0.003	4.04 ± 0.02	C
DTX	0.0887 ± 0.0002	11.78 ± 0.03	12.99 ± 0.03	0.958 ± 0.001	4.17 ± 0.02	E
DTX+CPP	0.0881 ± 0.0004	11.86 ± 0.05	13.08 ± 0.06	0.958 ± 0.001	4.17 ± 0.01	E
CBTXL	0.0897 ± 0.0008	11.7 ± 0.1	12.8 ± 0.1	0.960± 0.001	4.16 ± 0.03	E
CBTXL+CPP	0.0888 ± 0.0008	11.8 ± 0.1	13.0 ± 0.1	0.961± 0.001	4.16 ± 0.02	E
BIII	0.0978 ± 0.0001	10.68 ± 0.01	11.78 ± 0.01	0.958± 0.001	4.17 ± 0.01	E
BIII+CPP	0.0965 ± 0.0002	10.83 ± 0.02	11.94 ± 0.02	0.958± 0.001	4.18 ± 0.02	E
Azido-BIII	0.0983 ± 0.0003	10.63 ± 0.03	11.71 ± 0.04	0.960± 0.001	4.17 ± 0.01	E
Azido-BIII+CPP	0.0966 ± 0.0003	10.82 ± 0.03	11.92 ± 0.02	0.960± 0.001	4.17 ± 0.01	E
CTX40	0.0909 ± 0.0004	11.50 ± 0.05	12.67 ± 0.06	0.958± 0.001	4.18 ± 0.01	E
CTX40+CPP	0.0942 ± 0.0002	11.09 ± 0.02	12.23 ± 0.03	0.958± 0.001	4.18 ± 0.01	E
CTX101	0.0911 ± 0.0003	11.47 ± 0.04	12.64 ± 0.04	0.950± 0.004	4.21 ± 0.02	E
CTX102	0.0913 ± 0.0002	11.45 ± 0.02	12.62 ± 0.03	0.960± 0.001	4.16 ± 0.01	E
CTX102+CPP	0.0905 ± 0.0006	11.55 ± 0.08	12.73 ± 0.09	0.958± 0.001	4.17 ± 0.01	E
3´N-PT	0.0937 ± 0.0005	11.15 ± 0.06	12.29 ± 0.07	0.956± 0.002	4.18 ± 0.01	E
2-AB-PT	0.0925 ± 0.0003	11.30 ± 0.04	12.45 ± 0.04	0.957± 0.001	4.18 ± 0.01	E
2-AB-PT+CPP	0.0882 ± 0.0006	11.85 ± 0.08	13.06 ± 0.09	0.960± 0.006	4.17 ± 0.03	E
FTX1	0.0817 ± 0.0001	12.79 ± 0.02	14.10 ± 0.02	0.989 ± 0.001	4.04 ± 0.01	C
FTX1+CPP	0.0809 ± 0.0002	12.91 ± 0.03	14.24 ± 0.04	0.960± 0.001	4.16 ± 0.01	E
FTX2	0.0816 ± 0.0004	12.81 ± 0.06	14.12 ± 0.07	0.986 ± 0.001	4.06 ± 0.01	C
FTX2+CPP	0.0806 ± 0.0002	12.97 ± 0.03	14.29 ± 0.04	0.958± 0.001	4.17 ± 0.01	E
FCH3	0.0807 ± 0.0002	12.96 ± 0.03	14.27 ± 0.04	0.983± 0.001	4.07 ± 0.01	C
FB44	0.0831 ± 0.0004	12.58 ± 0.06	13.86 ± 0.05	0.986± 0.004	4.06 ± 0.02	C
FB44+CPP	0.0816 ± 0.0003	12.80 ± 0.05	14.11 ± 0.05	0.958± 0.002	4.17 ± 0.01	E
FB53	0.0877 ± 0.0002	11.92 ± 0.03	13.13 ± 0.03	0.987± 0.002	4.05 ± 0.01	C
FB53+CPP	0.0886 ± 0.0003	11.79 ± 0.04	13.00 ± 0.04	0.97 ± 0.01	4.12 ± 0.04	B
HXFTX	0.0824 ± 0.0001	12.68 ± 0.02	13.98 ± 0.02	0.99± 0.01	4.06 ± 0.01	C
HXFTX+CPP	0.0785 ± 0.0001	13.31 ± 0.02	14.67 ± 0.02	0.963± 0.002	4.15 ± 0.05	B
ATX	0.085 ± 0.003	12.3 ± 0.5	13.6 ± 0.5	0.988± 0.001	4.05 ± 0.01	C
ATX+CPP	0.0889 ± 0.0003	11.75 ± 0.04	12.96 ± 0.04	0.958± 0.001	4.18 ± 0.01	E

Table Ia. Structural parameters of microtubules in the presence of taxanes.

1.- nm^{-1}.
2.- nm as calculated from $J_{02}=1.045/R$.
3.- Calculated from an interprotofilament mean distance of 5.7 nm(35).
4.- C Compressed, E Expanded, B Blurred.
Abbreviations employed (see Figure 1): PTX: paclitaxel, DTX: docetaxel, CBTXL: cabazitaxel, BIII: baccatin III, Azido-BIII: 2m-azido-Baccatin III, CTX40: Chitax 40, CTX101: Chitax 101, CTX102: Chitax 102, 3'N-PT: 3´-aminobenzoyl paclitaxel, 2-AB-PT: 2-aminobenzoyl paclitaxel. FTX1: Flutax 1; FTX2: Flutax 2; FCH3: FChitax 3. HXFTX: Hexaflutax. ATX: alanylpaclitaxel.

Drug	J_{02}[1]	Radius[2]	Avg PF num[3]	1 nm^{-1} band	Avg monomer rise	State[4]
Epothilones						
Epo A	0.0939 ± 0.0001	11.13 ± 0.01	12.27 ± 0.01	0.960 ± 0.01	4.17 ± 0.01	E
Epo A+CPP	0.0931 ± 0.0004	11.22 ± 0.05	12.37 ± 0.05	0.959 ± 0.01	4.17 ± 0.01	E
Epo B	0.0910 ± 0.0002	11.48 ± 0.03	12.65 ± 0.03	0.962 ± 0.002	4.16 ± 0.01	E
Epo B+CPP	0.0923 ± 0.0005	11.32 ± 0.06	12.48 ± 0.07	0.963 ± 0.002	4.16 ± 0.01	E
Epo D	0.0926 ± 0.0003	11.29 ± 0.04	12.44 ± 0.04	0.966 ± 0.006	4.15 ± 0.03	E
Epo D+CPP	0.0926 ± 0.0004	11.29 ± 0.05	12.44 ± 0.05	0.957 ± 0.004	4.18 ± 0.02	E
IBP	0.0930 ± 0.0001	11.24 ± 0.01	12.39 ± 0.01	0.961 ± 0.001	4.16 ± 0.01	E
IBP+CPP	0.0913 ± 0.0008	11.4 ± 0.1	12.6 ± 0.1	0.960 ± 0.001	4.17 ± 0.01	E
Zampanolides						
ZMP	0.0793 ± 0.0002	13.17 ± 0.03	14.52 ± 0.04	0.988 ± 0.001	4.05 ± 0.02	C
ZMP+CPP	0.0785 ± 0.0002	13.31 ± 0.03	14.67 ± 0.04	0.986 ± 0.001	4.06 ± 0.01	C
DCT	0.0888 ± 0.0001	11.77 ± 0.01	12.97 ± 0.01	0.959 ± 0.001	4.17 ± 0.01	E
DCT+CPP	0.0881 ± 0.0004	11.86 ± 0.05	13.08 ± 0.05	0.958 ± 0.001	4.17 ± 0.01	E
TB282	0.10 ± 0.01	10.5 ± 1.1	11.5 ± 1.3	0.987 ± 0.001	4.05 ± 0.01	C
TMA282+CPP	0.0803 ± 0.0001	13.01 ± 0.02	14.35 ± 0.02	0.97 ± 0.01	4.12 ± 0.05	B
GS305	0.0793 ± 0.0001	13.18 ± 0.02	14.53 ± 0.02	0.987 ± 0.001	4.05 ± 0.01	C
GS305+CPP	0.0784 ± 0.0001	13.33 ± 0.02	14.69 ± 0.02	0.982 ± 0.007	4.07 ± 0.01	B
Discodermolide						
DDM	0.089 ± 0.003	11.7 ± 0.4	12.9 ± 0.4	0.988 ± 0.003	4.05 ± 0.02	C
DDM+CPP	0.0900 ± 0.0008	11.6 ± 0.1	12.8 ± 0.1	0.990 ± 0.003	4.04 ± 0.02	C
Cyclostreptin						
CSTR	0.0888 ± 0.0002	11.77 ± 0.03	12.97 ± 0.03	0.987 ± 0.001	4.05 ± 0.01	C
Taccalonolide						
TACCA-AJ	0.0902 ± 0.0002	11.58 ± 0.03	12.77 ± 0.03	0.987 ± 0.001	4.05 ± 0.01	C
Peloruside/Laulimalide						
LAU	0.0838 ± 0.0002	12.47 ± 0.03	13.75 ± 0.03	0.990 ± 0.003	4.04 ± 0.02	C
LAU+CPP	0.0842 ± 0.0002	12.41 ± 0.03	13.68 ± 0.03	0.97 ± 0.01	4.12 ± 0.05	B
PLA	0.0965 ± 0.0002	10.83 ± 0.03	11.94 ± 0.03	0.987 ± 0.001	4.05 ± 0.01	C
PLA+CPP	0.0981 ± 0.0004	10.65 ± 0.05	11.74 ± 0.05	0.958 ± 0.001	4.17 ± 0.01	E
PPH	0.0890 ± 0.0002	11.74 ± 0.03	12.94 ± 0.03	0.987 ± 0.001	4.05 ± 0.01	C
PPH+CPP	0.0906 ± 0.0001	11.53 ± 0.02	12.71 ± 0.02	0.959 ± 0.001	4.17 ± 0.01	E
CW235	0.0878 ± 0.0003	11.90 ± 0.04	13.12 ± 0.04	0.987 ± 0.001	4.05 ± 0.01	C
CW235+CPP	0.0872 ± 0.0002	11.98 ± 0.03	13.21 ± 0.03	0.958 ± 0.001	4.17 ± 0.01	E
Co-stabilized MTs						
PTX+LAU	0.0857 ± 0.0002	12.19 ± 0.03	13.44 ± 0.03	0.958 ± 0.001	4.17 ± 0.01	E
PTX+PLA	0.1002 ± 0.0003	10.42 ± 0.03	11.50 ± 0.03	0.954 ± 0.001	4.19 ± 0.01	E

Table Ib. Structural parameters of microtubules in the presence of other taxane and peloruside/laulimalide site ligands.
1.- nm^{-1}.
2.- nm as calculated from $J_{02}=1.045/R$.
3.- Calculated from an interprotofilament mean distance of 5.7 nm (35).
4.- C: compressed, E: expanded, B: blurred.
Abbreviations employed (see Figure 1): Epo: epothilone, IBP: ixabepilone, DDM: discodermolide, ZMP: zampanolide, DCT: dactylolide, CSTR: cyclostreptin; TACCA-AJ: taccalonolide AJ, LAU: laulimalide, PLA: peloruside A. PPH: pelophen B.

As expected from previous results (21, 33-36), ligand binding to both MSAs sites strongly
influences MT structure. From the images (**Figure 2**) obtained we can determine two different
clear effects on MT structure. The first and easier to interpret change occurs in the spacing of the
layer lines: in the presence of ligands, a new set of layer lines not visible in apo MTs can be easily
noticed at a spacing of 8 nm^{-1} from the equator, arising from the new 8 nm helix defined by ligand
binding to the MT lattice. Secondly, it can be noticed that, in the presence of some of the ligands,
the 4 nm^{-1} layer lines are displaced inwards, indicating that the microtubular lattice is expanded.
Interestingly, such expansion occurs asymmetrically and this allows to distinguish between α- and
β-tubulin as the set of layer lines at 8 nm^{-1} can also be noticed in the images. Interestingly, only
two possible dimer rise distances (4.06 or 4.17 nm) are possible, indicating two interchangeable
lattice spaces. It is worth noting that certain combinations of a drug stabilizing the compressed
state with GMPCPP result in blurred layer lines at intermediate spacings, which is indicative of
inhomogeneous lattices. This lattice expansion has been previously described upon binding of
paclitaxel and derivatives (34, 43), i.e., upon paclitaxel binding, the distance between α1- and β2-
tubulin subunits of two longitudinally aligned, concatenated tubulin dimers increases by roughly
2 Å relative to the unbound MT.

From the data obtained it can be noted that all taxanes, except those modified in C-7 (42),
and epothilones, induce lattice expansion. On the other hand, discodermolide, zampanolide,
cyclostreptin and taccalonolide AJ are able to stabilize MTs without having any effect on the
longitudinal spacing of the lattice, in common with compounds targeting the laulimalide/peloruside
site (e.g., laulimalide, peloruside A, pelophen B and CW235), and are in agreement with previous
results (25). These results indicate that it is also possible to stabilize MTs through the taxane site
without expanding them.

Another clear effect observed upon MT stabilization by MSAs bound at the taxane site is
the change in the position and shape of the J_0 maxima in the equator of the diffraction image.
Such changes indicate that binding to the taxane site influences lateral IPF interactions as it has
been previous described, both for the taxane site (33, 35) and the laulimalide/peloruside site (25).
However, although these results are concordant with previous studies—because paclitaxel
reduces the mean MT diameter while docetaxel keeps the MT diameter unaltered (33, 35)—it is
not straightforward to rationalize the observed changes.

From close examination of the fiber diffraction images the following facts can be deduced.
Firstly, as expected the position of the J_n peak remains unaltered, since it arises from the IPF
space and ligand binding is not expected to significantly alter the PF shape. Secondly, as a
general tendency those compounds that expand the microtubular lattice usually reduce or retain
the PF number, with baccatin III decreasing the MT radius to 10.32 ± 0.04 nm (average 11.38 ±
0.05 PFs). However, MSAs that do not expand the MT lattice do increase the MT radius; e.g.,
zampanolide increases the MT radius to 13.32 ± 0.04 nm (average 14.68 ± 0.05 PFs). Other
combinations of drugs with GMPCPP allow the generation of wider MTs with an expanded lattice.

257
Figure 2. Interpretation of microtubule diffractograms. A. Reference image illustrating
equatorial signal interpretation and Bessel peaks positions. **B.** Reference image illustrating
meridional signal interpretation and layer lines localizations. **C–F**. Representative diffractograms
for four microtubule conditions: (C) APO (gray), (D) PTX (light blue), (E) BIII (green), and (F) ZMP
(purple). **G.** Azimuthally integrated equatorial profiles from the diffractoACams above, including
theoretical ranges for Bessel J_0 peak positions corresponding to microtubules with radii between
10 and 15 nm. **H.** Azimuthally integrated meridional profiles focused on the 1 nm^{-1} layer line,
highlighting the ranges associated with compacted and expanded lattice states.
266

267
Figure 3. Relationship between the MT lattice state and MT radius for all the measured
conditions.

Stoichiometry of the taxane site regulation of the microtubule structure.

Having demonstrated that the occupancy of the paclitaxel site results in changes in the
microtubular lattice both in the longitudinal and the lateral directions, we aimed to understand the
stoichiometry needed to produce this effect (**Figure 4**) to learn the possible responses of axonal
MTs to different drug concentrations. We selected five taxane-site compounds, three of which are
in clinical use (paclitaxel, docetaxel and ixabepilone), another taxane engineered to be
fluorescent by a small modification at the C-13 side chain (3'N-PT), and the covalent binder
zampanolide. Paclitaxel, ixabepilone, and 3'N-PT expand the lattice in the longitudinal direction
while altering the IPF contacts which results in the loss of one PF on average (**Table I**); docetaxel
changes only the longitudinal spacing while zampanolide, a compound inducing a compressed
lattice, was tested on GMPCPP-bound pre-expanded MTs.

281
Figure 4. Structural response of microtubules to different ligand:tubulin ratios. The plots show the
variation in average monomer length and protofilament number, highlighting the impact of ligand
concentration on lattice organization. (A) paclitaxel, (B) docetaxel, (C) ixabepilone, (D)
3´aminobenzoyl paclitaxel, (E) zampanolide.

Remarkably, MTs are sensitive to the presence of substoichiometric concentrations of
drugs, i.e., all drugs are able to induce the structural transition towards its equilibrium state (those
obtained in fully bound MTs) at low saturation rates. Noticeable, transitions in both the longitudinal
and lateral directions behave as an almost all-or-nothing principle. Concerning the longitudinal
space transition, docetaxel- and 3'N-PT-bound MTs are expanded at the lowest stoichiometry of
the drug tested (0.33); paclitaxel and ixabepilone induced expansion as well, whereas

zampanolide induced re-compression of the GMPCPP expanded lattice at the 0.33–0.66
stoichiometry range.
294

Time-resolved fiber diffraction analysis of the structural effect of chemical stabilization of
microtubules induced by MSAs.

Once we examined the stoichiometry required to promote structural changes on MTs, we
investigated the ability of the MT to react to changes in the chemical composition of the
environment (**Supp. Movie 1**). To this end, we examined how three taxanes—docetaxel (PF-
neutral) and the thinner MT promoters paclitaxel and baccatin III—affect pre-formed MT lattices,
compared with laulimalide, an MSA that increases PF number without altering the axial tubulin
repeat (25).

Previous reports on time-resolved measurements of the mean diameter of non-aligned
MTs indicate that the change in diameter in response to the addition of paclitaxel or docetaxel
occurs within the dead time of the technique, i.e., 30 s (44) (note that our shear flow and mixing
system allows a time resolution of 1 s). Our findings presented in **Figure 5** reveal that upon
addition of paclitaxel, docetaxel or baccatin III, the axial expansion of the MT takes place in less
than 1 s. The consistency of this result is suggestive of a flexible lattice that is able to rapidly
expand in response to the occupation of the taxane site by an expanding drug. The control
experiment in the presence of the non-expanding MSA laulimalide shows no change upon drug
addition (**Figure 5D**).

On the other hand, modification of the lattice in the lateral direction is, although slower in
concordance with previous reports (44), far less extensive (at least in the early stages) than
expected from the static measurements. Paclitaxel-induced microtubules contained, on average,
0.6 fewer PFs than those assembled in the absence of the drug. However, only a reduction of 0.3
PFs was observed during the first 3 s of measurement. Prolonged exposure (30 min) of
preassembled microtubules to superstoichiometric concentrations of paclitaxel resulted in MTs
apparently identical to those assembled in the continuous presence of the drug.

Figure 5. Time-resolved axial and radial measurements reveal different dynamics of microtubule
lattice reorganization after ligand addition at 40 s (red dashed line). Left: average axial tubulin
repeat. Right: average protofilament number. Ligands: (A) paclitaxel, (B) docetaxel, (C) baccatin
III, (D) laulimalide.

Baccatin III is the compound that promotes a larger modification in the IPF contacts with

a net loss of 1.1 PF. Similarly, for paclitaxel only a minor change of 0.3 PF was observed

immediately after addition.

Finally, adding laulimalide to pre-formed MTs was neutral for the dimer length, as

expected from previous results (25), and induced a net increment of 0.3 PF. Note that laulimalide

generates MTs with an average of 1 extra PF compared with the apo ones. In all cases shown

the time-resolved experiments revealed a fast small change in the PF number, indicating that the

equilibrium in this parameter takes place in a longer time scale.

'In silico' model building and simulation.

To understand the structural mechanisms responsible for taxane site ligands modulation

of the MT lattice and GTPase activation we next used computational modeling and molecular

dynamics (MD) simulations. Our aims were to study (i) the low-frequency motions involved in the

cooperative structural fluctuations leading to PF number variation in MTs, (ii) the conformational

behavior of a set of representative drug-free and drug-bound (docetaxel, epothilone A,

zampanolide, discodermolide and alatax) $\beta1:\alpha2$ interfaces from MTs differing in interdimer rise

and PF number, and (iii) the dynamics of a series of minimalist representations of MT lattices (45)

made up of three laterally associated PF fragments, each consisting of a dimer of αβ-tubulin

dimers. The results obtained allowed us to build several instances of representative full MT turns

with both compacted and expanded drug-bound lattices that are now publicly available from the

ModelArchive repository (46) (codes are listed in the Materials & Methods section).

The normal mode analyses performed on the 3´2 patches of tubulin dimers from 13- and

14-PF MTs consistently showed that the first non-trivial mode corresponds to a collective motion

that can nicely explain the large-amplitude, slow-bending motion that drives the cooperative

structural fluctuations justifying the observed PF number variation (**Supp. Movie 2**). By saving

the coordinates of the model corresponding to the maximum amplitude, we obtained a suitable

template for an [(α1:β1-α2:β2)/(α1':β1'-α2':β2')/(α1":β1"-α2":β2")] MT patch with either a slightly

higher or a slightly lower degree of closure that led, upon careful energy refinement, to MTs

consisting of 12 and 15 PFs, respectively.

Comparison of the $\beta1:\alpha2$ interfaces in the presence of either GTP (pre-hydrolysis state)

or GDP (post-hydrolysis state) in the β subunit clearly showed the expected direct interactions

between the γ-phosphate of the former and the T3 loop in place of the water-mediated interactions

with the β-phosphate in the latter. In addition, the simulations revealed a pleomorphic interface

that can subtly change in response to environmental cues, including the presence of magnesium

ions and the degree of solvation, which can give rise to distinct and easily interconvertible

hydrogen-bonding patterns that subtly modulate not only the lattice parameters but also the water

network and the torsion angles of the nucleotide distal phosphates (**Figure 6**). Most notably, the

Aspβ179 residue in the [177]VS<u>D</u>TV[181] stretch from the T5 loop, which in the PF adopts the so-

called "in" conformation (47) also found in the α-tubulin [177]VSTAV[181] counterpart, can accept a

hydrogen bond from the hydroxyl of Tyrβ224 (the first residue in H7 whose replacement by Phe

is known to promote the formation of straight tubulin oligomers, which are more efficient in

initiating MT nucleation and elongation (47)), the ribose hydroxyls of GTP, the Lysα352 amino

group, the backbone nitrogen of Valα353, and/or the sidechain carboxamide of Asnα329. The

Lysα352 amino group can also form a strong ionic interaction with the catalytic carboxylate of

Gluα254, which in turn can fixate the sidechain carboxamide of Asnβ101. This functionality allows

the formation of hydrogen bonds not only with Thrβ180 in the T5 loop but also with Asnα258

across the interdimer interface; besides, in concert with the backbone amide nitrogen, the

Asnβ101 carboxamide appears to be essential for orienting the γ-phosphate in the elusive

conformation that is necessary for nucleophilic attack by the activated water molecule (**Figure 6**).

Figure 6. Overlay of the β1-α2 interfaces from a compressed PF (light and dark pink) with bound
discodermolide (C atoms in orange) and an expanded PF (light and dark gray) with bound
paclitaxel (C atoms in green) using only the β1 subunits for the root-mean-square superposition
in PyMOL. The interdimer rise, measured as the distance between the centers of mass of the Cα
atoms of β and α subunits, is 40.5 Å for the former and 42.0 Å for the latter. The C atoms of the
GDP and GTP nucleotides are colored yellow and salmon, respectively, and the Mg^{2+} ions are
displayed as green spheres. The boxed area appears enlarged at the top of figure to show the
most notable interfacial differences and the hydrating water molecules (cyan thin sticks). Relevant
residues explained in the text have been labeled.

Optimization of this intricate interplay is only achieved when the GTP cap matures and,

as shown here, is amenable to modulation by MSAs bound at the taxane site. These bound

ligands change the vibrational patterns and contribute to these conformational fluctuations in

slightly different ways depending on their chemical nature and the specific anchor residues
involved. The present results support the proposed crosstalk between the nucleotide- and taxane-
binding sites.
392
393   ***Effect of microtubule structure on nucleotide hydrolysis.***
394   Considering that MSAs are able to regulate the average monomer rise and the GTPase
activity at the E-site in β-tubulin, which is activated by the Gluα254 residue of the incoming tubulin
dimer (48), we aimed to investigate whether the modulation of the tubulin structure by MSAs is
reflected into differences in GTPase activity. To this end, we compared the GTPase activity of
MTs in the presence of a set of expanding (paclitaxel, epothilone A) and non-expanding ligands
bound to the taxane (discodermolide, zampanolide) or laulimalide/peloruside sites (pelophen B)
(25) relative to that of undrugged ones.
401   Firstly, we confirmed the GTPase activity of drugged MTs by analyzing the nucleotide
content of the assembled polymers. All drugged MTs were found to have 1 mole of GTP and 1
mole of GDP bound per tubulin dimer at one hour of incubation, indicating retention of GTPase
activity. Then, phosphate release was quantified using the malachite green inorganic phosphate
assay (49) (**Table II**). These results indicate, in concordance with previous reports (50), that
expansion reduces the kinetic rate of phosphate release by nearly 35%, while discodermolide
binding increases the hydrolysis rate by 45%.
408

Condition	Kinetic rate of phosphate release (min^{-1})
Apo (C)	0.11 ± 0.02
Paclitaxel (E)	0.07 ± 0.01
Epothilone A (E)	0.07 ± 0.02
Zampanolide (C)	0.11 ± 0.03
Discodermolide (C)	0.16 ± 0.02
Pelophen B (C)	0.10 ± 0.02

409
410   **Table II**. GTPase activity of drugged expanded and compressed microtubules. (C) compressed
411   and (E) expanded state of tubulin.
412
413   The finding that GTP hydrolysis is slower in expanded MTs (i.e., bound to paclitaxel or
epothilone A) and faster in MTs with bound discodermolide is indicative of an optimal alignment -
in the latter case of the Gluα254-activated water molecule that performs the nucleophilic attack
on the γ-phosphate to cleave the bond between the γ- and the β-phosphate (**Figure 6**). This
reaction has been deemed to be, on theoretical grounds (51), extremely sensitive to the
geometrical features of the site and this assertion is confirmed by the present results, which show
that activation of GTP hydrolysis at the E-site is distinctly regulated by ligands. Intriguingly, binding
of the pseudocyclic discodermolide—despite its deceitfully greater conformational freedom on
paper relative to its macrocyclic congeners, e.g., dictyostatin)—displays an unusual favorable
entropic contribution to the binding free energy (52). On the basis of our MD simulation results for
both the free and bound forms, we posit that its high binding affinity for tubulin is achieved by

significant conformational restraints—mostly due to the distinct distribution of double bonds—that
pre-shape this ligand to exhibit excellent shape and electrostatic complementarity with the taxane
binding site on the β-tubulin subunit of straight PFs without incurring in strain and entropic
penalties. Furthermore, the hydroxyl groups that point outward interact, in a very precise fashion,
with both donor/acceptor groups in the taxane binding pocket, and also with some water
molecules. This binding signature is unique to discodermolide, as it involves the side chains of
Aspβ226 and Hisβ229 in helix H7, the backbone nitrogen of Thrβ276, the backbone carbonyl of
Argβ369 in the T9 hairpin and the carboxamide group of Glnβ281 in the M loop. As a result of the
vibrational changes brought about by this anchoring, the bound drug elicits an allosteric effect on
the conformation of the GTP phosphates at the E-site such that the attack by the Gluα254-
activated nucleophilic water molecule is facilitated and the interdimer rise shortening is promoted.
On the contrary, taxane and epothilone binding, by establishing a different well-described set of
interactions (21, 53), increase the interdimer rise distance and slow down the GTP hydrolysis rate
because they promote an alternative arrangement of the GTP phosphates that raises the energy
barrier that is necessary to overcome in order to stabilize the transition state of the reaction.
439
Effect of structural changes on chemical transport on microtubules.
Kinesin-mediated chemical transport, crucial for neurotransmitters movement along the
axons, is one of the main cellular functions of microtubules (54). This transport relies on kinesin
recognition of the MT surface. Now that we have the tools to modulate MT structures, we aim to
understand how these structural changes affect kinesin motility.
To address this issue, we employed the time-lapse total internal reflection fluorescence
(TIRF) microscopy system described in our previous study (42). Using labeled kinesin motors
(Kif5B 1–905-eGFP (55)), we tracked and analyzed individual kinesin particles upon immobilized
MTs stabilized by a panel of distinct MSAs that produce different architectures, to characterize
several physical properties (**Figure 7 and Supp. Movie 3**) related with their function
(affinity -motors per unit MT length-, run length, interaction time, and average velocity). Data for
paclitaxel (expanded, reduced PF number), FB44 (compressed, increased PF number), FB53
(compressed, neutral PF number), and GMPCPP (expanded, neutral PF number) were taken
from our earlier work (42). We then selected four additional compounds targeting the taxane site—
docetaxel (expanded, neutral PF number), epothilone B (expanded, reduced PF number),
zampanolide (compressed, increased PF number), and discodermolide (compressed, neutral PF
number)—and three compounds targeting the peloruside/laulimalide site—peloruside A
(compressed, reduced PF number), laulimalide (compressed, increased PF number), and
pelophen B (compressed, neutral PF number).
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Figure 7. Characterization of kinesin motility. A. Schematic representation of the single-
molecule kinesin motility assay. Stabilized microtubules (MTs) were immobilized in a pre-treated
flow chamber, and 10.8 nM Kif5B-eGFP was added. The movement of individual motors was
recorded using TIRF microscopy and subsequently analyzed. **B–E.** Scatter plots and quantitative
summary from at least three independent experiments, showing (B) mean landing rate of kinesin
(events/µm per s), (C) mean dwell time (s), (D) mean run length (µm), and (E) mean velocity
(µm/s) of single Kif5B-eGFP molecules moving on stabilized MTs. Error bars represent the SEM.
Data were pooled from ≥ 2 experiments per condition, analyzing between 36–48 MTs per replica.
F. Representative kymographs of single Kif5B-eGFP motors moving along a stabilized
microtubule. Vertical scale bar: 2 µm; horizontal scale bar: 10 s.
471

Figure 8. Statistical correlations found between the structural and affinity parameters of the drug-stabilized lattices and the interaction of kinesin with them. Pearson correlation was obtained using GraphPad Prism 8 software to determine R square and P value (**** $p < 0.0001$; *** $p < 0.001$, ** $p < 0.01$ and * $p < 0.05$).

Although the data presented here demonstrates a complex dependence of kinesin–MT interactions on the specific structural state induced by drug binding, overall, it confirms that ligand binding to MT alters kinesin interaction and motility. Hence, we have identified several consistent trends. Firstly, the velocity (**Figure 7E**) can be categorized as faster and slower, and correlates with the monomer length state (**Figure 8A**), being consistently faster on expanded lattices (as kinesin-decorated MTs are typically expanded) and on lattices stabilized by ligands with relatively low binding affinities (FB44, FB53, and PPH). In contrast, strongly stabilized compressed lattices yield slower motility. This may reflect that low binding affinity ligands poorly stabilize the compressed state, making kinesin binding induced expansion easier. Landing rate (**Figure 7B**) is reduced on expanded lattices and in the presence of zampanolide (which increases PF number). The interaction time (**Figure 7C**) is generally consistent across conditions, except for epothilone B, which produces significantly shorter dwell times. The run length (**Figure 7D**) is relatively stable across conditions, with two notable exceptions: epothilone B, which reduces run length, and PPH, which increases it. Interestingly, the run length correlates to some extent with the affinity of the assayed ligands (**Figure 8B**), suggesting that stronger stabilization of the microtubule impairs kinesin-movement-associated accommodation of the lattice during kinesin's functioning.

It is worth mentioning that epothilone B stands out as the only compound that strongly stabilizes an expanded lattice ($K_b = 1.5 \times 10^9$ M^{-1} at 26 °C). Despite kinesin moving at the same velocity on epothilone B-stabilized lattices, it binds with lower affinity and dissociates more rapidly compared to other conditions.

Effect of structural changes on tau binding and kinetics.

Tau is the most important MT modulator in axons, requiring a highly dynamic interaction with MTs to exert its stabilizing function (56). Failure of tau to interact with MTs leads to the formation of neurofibrillary tangles—typical of Alzheimer disease—in addition to the impaired stability of axonal MTs. In order to learn from the structural features influencing tau recognition by MTs, we employed the same drugs as kinesin binding assay to study the interaction of mCherry

Figure 9. Characterization of tau interaction with microtubules. A. Schematic representation
of the TIRF microscopy assay setup. Label-free stabilized microtubules (MTs) were immobilized
on a pre-treated glass coverslip. Purified tau-mCherry was added, and its binding to MTs was
recorded. Fluorescence intensity of tau-mCherry along each MT was measured and analyzed. **B.**
Representative fluorescence images (after 4 minutes) and corresponding kymographs of tau-
mCherry binding to MTs stabilized with GMPCPP or different drugs. Vertical scale bars: 2 μm;
horizontal scale bars: 60 s. Taxol derivatives are shown in blue shades, other taxanes in purple
tones, and peloruside/laulimalide site ligands in different greens. Triangle symbols indicate
expanders; circle symbols represent non-expander compounds. **C.** Fraction of MT length covered
by tau envelopes over time following tau-mCherry addition. **D.** Integrated fluorescence density
per μm of MT over time after tau-mCherry addition.

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520

A   Correlation of MT size vs % coverage

B   Correlation of lattice state vs % coverage

R square 0.3351
P value *
R square (Exc PLA and DDM) 0.6811
P value **

R square 0.8219
P value ****

C   Correlation of MT size vs IntDen/µm

D   Correlation of lattice state vs IntDen/µm

R square 0.4196
P value *
R square (Exc PLA and DDM) 0.7639
P value ***

R square 0.7546
P value ***

Figure 10. Statistical correlations found between the structural parameters of the drug stabilized lattices and the binding of tau to them. Pearson correlation was obtained using GraphPad Prism 8 software to determine R square and P value (**** $p < 0.0001$; *** $p < 0.001$, ** $p < 0.01$ and * $p < 0.05$).

labeled tau 441 isoform with immobilized stabilized MTs, using the same technique as we performed in our previous work (42).

We deposited the distinct ligand-bound stabilized MTs in a flow chamber and visualized them using total internal reflection microscopy. We then added 10 nM of tau-mCherry and monitored its association with MTs (**Figure 9A**). As for zampanolide, discodermolide, peloruside A and laulimalide, the standard tau concentration of 10 nM resulted in instantaneous binding that precluded any kinetic analysis we reduced the initial tau concentration to 5 nM to resolve whether tau binding occurred uniformly along the microtubule or binding proceed through patches that grow at an accelerated rate.

After 4 min, we increased the tau-mCherry concentration up to 10 nM for zampanolide, discodermolide, peloruside A and laulimalide and up to 40 nM for the rest of the ligands, recording its binding to MTs for another 4 min. Data for GMPCPP, paclitaxel, FB44 and FB53 are taken from(42).

The most relevant observation is that zampanolide-, discodermolide- and laulimalide-stabilized
MTs bind tau within the dead time of the technique (MTs are fully covered in 10 seconds) despite
the lower concentration of tau employed (5 nM instead of 10 nM), suggesting that these structures
are very easily recognized by tau (**Figure 9B**, **9C** and **Supp. Movies 4–6**) while GMPCPP MTs
are not covered, indicating that this lattice is not recognized by tau. Concerning the other
stabilized MTs, we observed that tau bound in patches which diffused along MTs expanding
progressively as previously described for tau binding to them (57). In good agreement with
previous results (42), expanded MTs (epothilone B- and docetaxel-bound) bind tau with rates
similar to those observed for paclitaxel-bound MTs (42), requiring times in the order of minutes to
significantly cover MTs (**Supp. Movies 7** and **8**). Although there is a clear correlation between
lattice expansion and tau binding (**Figure 10B** and **10D**), there are clear differences between
binding of tau to different non-expanded lattices. Zampanolide, discodermolide, and laulimalide
stabilized MTs within the dead time of the technique (fully covered in 10 s), peloruside A- and
pelophen B-stabilized MTs bind tau noticeably slower (**Supp. Movies 9** and **10**) (although faster
than expanded MTs), behaving similar to MTs stabilized by taxanes in which the expansive effect
had been removed by the addition of groups at C-7 position (42).

We also calculated the total amount of tau bound to the structures (**Figure 9D**) based on
the total fluorescence signal. The clear distinction in this measurement between expanded and
non-expanded lattices resembles the percentage of MT cover (**Figure 9B**). While expanded MTs
(paclitaxel, docetaxel and epothilone B) require 40 nM tau-mCherry and a long exposure time to
show an average fluorescence over the background, compacted lattices bind rapidly to reach a
full binding at lower times and concentrations. However, it is worth mentioning that although tau
covers all the zampanolide-, discodermolide- and laulimalide-stabilized MTs within the dead time
of the technique, with pelophen B and peloruside A showing slower binding kinetics, full binding
of tau is not immediate as the MT continuously increases fluorescence with time until it reaches
the maximum value.

Finally, it is not possible to find a strong correlation between MT diameter and tau binding,
albeit a weak correlation (with outliers) can be observed, inferring that thicker MTs allow to bind
a higher concentration of tau (**Figures 10A** and **10C**). Collectively, these observations together
with the evidence that tau affinity correlates with lattice state, are consistent with fact that MTs
stabilized by expanding drugs are thinner than those stabilized by non-expanding drugs (see
above).

Discussion

The discovery of taxanes and their biomimetics opened the possibility of blocking the
cytomotive switch in the straight microtubule (MT) conformation (21). By stabilizing MTs in this
state, these compounds prevent the generation of pulling forces and, consequently, the
segregation of sister chromatids during mitosis, while maintaining the structural integrity of the
microtubule network. In principle, such an approach to tubulin-targeted therapy should inhibit cell
division and angiogenesis without compromising the structural functions of MTs in axons.

Therefore, it was initially expected to cause less neurotoxicity than vinca alkaloids and other
microtubule-destabilizing agents (MDAs), whose mechanisms of action rely on MT
depolymerization (19). However, after their clinical approval in 1992, paclitaxel and other MSAs
targeting the paclitaxel site—docetaxel, cabazitaxel, and ixabepilone—were shown to induce
stronger and more persistent neurotoxic effects than vinca domain–binding drugs (23, 24). Early
structural studies revealed that paclitaxel-induced MT stabilization occurs at the cost of lattice
perturbation (33, 35), and that the addition of paclitaxel to preassembled MTs leads to changes
in the number of PFs (44). Given that structural features are critical for MAP recognition and
binding (1, 26), it is reasonable to propose that the observed neurotoxicity—and its long-lasting
nature—arise from altered microtubule architecture induced by these drugs.

Building upon our previous work (21, 25, 34), which demonstrated that nearly all drug-
mediated MT stabilization occurs at the expense of structural distortion, we sought to investigate
in depth the structural consequences of MSA-induced microtubule stabilization.

Microtubule structure is primarily defined by two parameters—the helical pitch and the
diameter—which together determine the overall lattice geometry. A third structural parameter, the
PF twist, cannot be resolved by fiber diffraction. The helical pitch reflects the average monomer
length, while the diameter is determined by the number of PFs. We observed a binary behavior
in the monomer length, which adopts only two distinct states: compressed (4.06 nm) or expanded
(4.17 nm). Compounds containing a taxane core expand the lattice from the apo (4.06 nm) to the
expanded (4.17 nm) state, as previously described for GMPCPP (37, 39), paclitaxel, docetaxel,
and related derivatives (21). The same behavior is observed for epothilones, whereas other
chemotypes that bind to the paclitaxel site—such as discodermolide, zampanolide, cyclostreptin,
and taccalonolide—or those binding to the laulimalide/peloruside site, do not induce lattice
expansion.

Together with previous results (21), these findings indicate that lattice expansion is neither
linked to occupancy of the taxane site nor to stabilization, as baccatin III, a non-stabilizing taxane
also expands the microtubule lattice. Expansion is not related to the molecular size of the ligand,
since both bulky (paclitaxel, docetaxel) and less bulky (epothilones, baccatin III) compounds
induce this effect. Moreover, the longitudinal expansion prompted by taxanes is abolished in the
presence of small C-7 modifications (for example, alatax), even though in this case the observed
compression can be reversed upon addition of GMPCPP. Interestingly, taxanes and
epothilones, despite their distinct interactions with Aspβ226 and Hisβ229 in H7, share a key
anchoring point because both chemotypes accept a hydrogen bond from the backbone nitrogen
of Thrβ276, located immediately before the M-loop, which is crucial for establishing lateral
contacts between neighboring PFs within the microtubule lattice (**Figure S1**). Nonetheless,
hydrogen bonding to Thrβ276 is also used by compactness-promoting ligands such as
zampanolide (which forms a covalent adduct with Hisβ229 in H7) and discodermolide (whose δ-
lactone accepts a strong hydrogen bond from Nε of Hisβ229) although these drugs also act as
hydrogen bond donors to this residue. On the contrary, taccalonolide AJ binds covalently to the
carboxylate of Aspβ226, does not hydrogen bond to Thrβ276, and does not promote expansion.

It is worth noting that Aspβ226 and Hisβ229 lie on one side of H7, facing the taxane site, whereas Tyrβ224 and Asnβ228 face the nucleotide at the E-site on the opposite side of the helix. Therefore, small changes in the orientation or straightness of H7 may be propagated between the E-site and the M-loop, thereby influencing both PF compactness and lateral associations in a ligand-dependent manner. Thus, H7 likely acts as a transducer that communicates structural signals between the taxane-binding site and the E-site so that the nucleotide phosphates can adopt alternative conformations and this, in turn, affects the β-tubulin T3 and T5 loops and the α-tubulin T7–CH8 region.

Strikingly, although C-7-modified taxanes and laulimalide/peloruside-site ligands compact the lattice, they still allow expansion in the presence of GMPCPP at the E-site of β-tubulin. In stark contrast, discodermolide and zampanolide stabilize the compacted conformation even in the presence of GMPCPP. This resistance to expansion likely reflects the exceptionally high binding affinity of discodermolide and the covalent nature of zampanolide binding, both of which override the typical expanding effect of GMPCPP probably by enforcing the conformational state that is most favorable for their optimal interaction. The likely importance of the diverse interactions with Thrβ276 is reinforced by the finding that dactylolide, a precursor of zampanolide that lacks the specific amide side chain, produces an expanded lattice.

Taken together, these findings strongly suggest that the compacted and expanded lattice states are energetically close, and that minimal chemical modifications can switch between them. This structural plasticity provides a mechanism for transmitting chemical signals through the lattice. It is also important to note that fluorescent probes can themselves alter microtubule conformation, a factor that should be carefully considered when selecting probes. Among those tested (**Table I**), two aniline-based probes (3´N-PT, 12.3 PF; and 2-AB-PT, 12.5 PF) stabilize the expanded conformation, whereas those containing C-7-linked fluorophores (FTX1, 14.1 PF; FTX2, 14.2 PF; FCH3, 14.3 PF; and HXFTX, 14.0 PF) stabilize compacted lattices.

Interpreting changes in mean microtubule diameter (i.e., PF number) in terms of ligand chemotype is more complex. Nonetheless, compounds that induce lattice expansion typically cause only moderate alterations in microtubule diameter, producing small adjustments in PF number (33, 35). The maximal changes observed are a loss of up to 0.6 PFs (1.2 PFs in the case of baccatin III) or a gain of 0.2 PFs. Conversely, taxane-site ligands that stabilize the compacted state tend to increase the PF number by up to 1.6. Peloruside/laulimalide-site ligands stabilize highly compacted microtubules with an average of 11.8 PFs (Estévez-Gallego, 2023 #3257), while GMPCPP promotes expansion even in large PF-number microtubules. By combining GMPCPP with different drugs, compressed microtubules can range from 11.8 PFs (peloruside A) to 14.5 PFs (zampanolide), and expanded microtubules from 11.5 PFs (peloruside A and paclitaxel) to 14.6 PFs (hexaflutax and GMPCPP).

These results illustrate how relatively subtle perturbations at the interdimer or IPF interfaces induced by stabilizing ligands translate into significant, measurable differences in MT compactness and PF number, as quantified by the methods described here and in previous studies (25, 34, 41, 58). Our modelling studies indicate that as discussed previously (59, 60), the

stabilization of lateral contacts between PFs that leads to the curved-to-straight conformational
transition relies on a loop-mediated latch model in which Hisα283 and Tyrβ283 in the M-loops of
α- and β- subunits, respectively, play the role of a rotating bolt and the H1-S2/H2-S3 of the lateral
partner act as the stationary keepers (**Figure 11**). In the case of the β-subunit, besides the
hydrogen bond between O(Tyrβ283) at the minus end of the M-loop helix and NH(Argβ88) in the
neighboring β-tubulin subunit, our modeled complexes reveal another hydrogen bond between
O(Glnβ282) in the M-loop and NH(Alaβ57) in the 56–59 twisted β-hairpin of the neighboring β-
tubulin subunit. Conceivably, this interaction network is sensitive to the presence of a bound ligand
in the taxane-binding site in such a way that the spatial relation between the M-loop
(278RGSQQY283) in one β-tubulin subunit and the twisted β-hairpin (53YNEAAGNKYV62) of the
β-subunit in the neighboring PFs changes slightly but sufficiently to act as a wedge that can either
increase or decrease the interPF angle and thereby lead to MTs with a higher or lower number of
PFs. Furthermore, since helix H7 and the following T7 loop in β-tubulin link the intra- and
interdimer interfaces where the bound nucleotide resides, the distinct interactions of taxane-site
ligands with the exposed side chains of Aspβ226 and Hisβ229 in helix H7 are likely to have an
impact on the rate of GTP hydrolysis, as reported here for paclitaxel, epothilone A and
discodermolide.

Figure 11. Overlay of 50 snapshots obtained from the cooling phase of the molecular dynamics
simulation of the β1-α2 interface in a protofilament with paclitaxel bound at the taxane site of the
beta subunit between helix H7 and the M-loop. The diagrammatic cylinder/stub representation
was obtained with ChimeraX v.1.10 and depicts the spatial relation between nucleotide- and
drug-binding sites. The side chains of His283 in the α-subunit and Tyr283 in the β-subunit act as
latches to reinforce the IPF interactions involving the H10-S2 and H2-S3 loops of tubulin
molecules in the neighboring PF.

Moreover, the results obtained for discodermolide highlight the importance of exploring
the three-dimensional conformational landscape of "linear" ligands in aqueous solution to assess
their true structural preferences and the potential for preorganization, as previously proposed to

explain the high antitumor potency of a linear zampanolide analogue (61). These examples
challenge the traditional medicinal chemistry notion that increased conformational flexibility is
necessarily detrimental to protein-binding affinity and biological activity.

The structural changes observed here underscore the remarkable plasticity of tubulin,
which can assemble into multiple polymeric forms (microtubules, sheets, rings, and others) by
accommodating distinct longitudinal and lateral contacts (27, 62). Although it was already known
that microtubules can modify their architecture in response to changes at the nucleotide (37, 39,
63), taxane (21, 44), and laulimalide/peloruside sites (25), the timescale required for structural
rearrangements in assembled polymers was previously unknown. Our data shows that co-
assembly or post-assembly drug addition produces the same final state with respect to lattice
expansion or compaction, whereas changes in PF number require considerably longer
equilibration times and do not yield perfectly identical structures (42).

Since ligand binding to the luminal taxane site is extremely fast (64-66), the rate-limiting
step for these structural transitions must be the intrinsic flexibility of the microtubule lattice. As
shown in **Figure 5,** the longitudinal expansion induced by compounds promoting the expanded
state occurs almost instantaneously—within the temporal resolution of our measurements—
whereas changes in PF number are comparatively slower (44), consistent with the energetic cost
of adding or removing PFs from an existing lattice.

Another long-standing question in the field concerns the stoichiometry of drug binding
required to alter microtubule structure. Because drug dosage varies in clinical use, the degree of
taxane-site occupancy may differ among treatments. Our results indicate that the structural
transition occurs at low saturation levels: 0.4–0.6 for paclitaxel and ixabepilone, and below 0.4 for
docetaxel. The transition appears to be binary, with no intermediate states detected. These
observations illustrate that the energetic difference between the compacted and expanded lattice
states is minimal and that the conformational transitions occur rapidly, consistent with their
proposed role as structural signals for protein-protein recognition. Environmental chemical
changes induced by small molecules can thus be transduced into microtubule structural
rearrangements, modulating their biochemical and mechanical properties. For example, we found
that microtubule-expanding drugs as paclitaxel and epothilone A significantly reduce the rate of
nucleotide hydrolysis, which could contribute to enhanced stabilization. Conversely,
discodermolide—because of its unique high-affinity binding mode—not only stabilizes
microtubules but also markedly accelerates nucleotide hydrolysis.

Finally, we examined how the structural determinants of MT lattices influence recognition
and function of two key MAPs: kinesin and tau. We found that drug binding alters kinesin motility
(**Figure 7**), with distinct effects depending on the lattice state—expanded or compressed—
induced by each ligand. Kinesin velocity is higher on expanded lattices and in the presence of
lower-affinity stabilizers (FB44, FB53, pelophen B), but slower on strongly stabilized compressed
lattices. Landing rates decrease on expanded lattices and in zampanolide-stabilized MTs, which
also show an increased number of PFs. Interaction times (dwell times) remain broadly similar
across conditions except for epothilone B, which shortens them. Run lengths are largely

unaffected, with the exceptions of epothilone B (decrease) and pelophen B (increase). These
results suggest that the tested drugs modulate kinesin–lattice interactions by reshaping the
energy landscape of stepping and binding: expansion combined with weaker stabilizers facilitates
stepping (faster motion), whereas strong compression hampers progression (slower motion).
Notably, epothilone B decouples velocity from binding stability—although the lattice is expanded,
its lower on-rate and shorter dwell time yield briefer runs despite maintained speed.

Regarding tau, we observed a clear preference for compressed lattices, regardless of
ligand chemotype, consistent with previous results from our group with taxanes (42). However,
marked differences arise depending on the stabilizing ligand. Tau binding is almost instantaneous
for MTs stabilized by zampanolide (14.5 PF, compressed), laulimalide (14.0 PF, compressed),
and discodermolide (12.9 PF, compressed), whereas it is significantly slower for those stabilized
by peloruside A (11.9 PF, compressed), pelophen B (13.0 PF, compressed), flutax-2 (13.7 PF,
compressed (42)), and other C-7-modified taxanes such as FB44 (13.6 PF, compressed) and
FB53 (12.8 PF, compressed (42)). These differences likely stem either from the distinct positions
of their binding sites (the taxane site lies within the MT lumen, whereas the laulimalide/peloruside
site is on the MT surface) or from the differential impact of the long side chain on local lattice
organization.

Conversely, tau binds expanded lattices at a much slower rate. In this study, we examined
two expanding chemotypes—docetaxel (13.0 PF, expanded) and epothilone B (12.7 PF,
expanded)—and obtained results consistent with previous data for paclitaxel (12.3 PF, expanded
(42)). Overall, the slowest tau binding was observed for docetaxel-stabilized MTs. These results
reinforce the clear preference of tau for compressed over expanded lattices, as reported
previously (67, 68). The observation that tau forms cohesive envelopes support that the
cooperative mechanism in which the lattice itself adjusts to accommodate tau's conformational
preferences. Nevertheless, in line with earlier studies, GMPCPP-expanded lattices are unable to
undergo such adaptation.

Analysis of the tau binding kinetics (**Figure 9**) reveals three characteristic different
behaviors depending on the bound drug. First, in MTs stabilized by zampanolide, laulimalide, or
discodermolide, tau rapidly decorates the entire filament within seconds, continuing to bind until
saturation. This indicates that these lattices are preorganized for tau recognition, requiring little or
no conformational rearrangement during binding. Second, in other compressed lattices, tau
envelopes form rapidly and subsequently grow, implying that these MTs can easily convert into
the tau-preferred conformation. Third, in lattices expanded by paclitaxel, docetaxel, or epothilone
B, tau binds diffusively and forms envelopes only slowly at high tau concentrations. This behavior
suggests that tau competes with the bound stabilizers, locally displacing them and creating
compacted patches that gradually expand as tau remodels the lattice. Finally, GMPCPP-stabilized
lattices, where the stabilizing agent is non-exchangeable, remain locked in an expansion state
that prevents conversion to a tau-binding conformation.

In this study, we have used our extensive library of MSAs to construct a comprehensive
structural atlas of tubulin modulation by small molecules. We demonstrate that low site occupancy

by distinct chemotypes allows fine-tuned control of MT architecture, enabling immediate and
reversible modulation of lattice conformation upon drug binding. These structural alterations
directly influence fundamental MT properties such as GTP hydrolysis rates and MAP interactions,
particularly those of kinesin and tau. This introduces a previously unrecognized layer of control,
positioning MSAs not only as stabilizing agents but also as molecular tools for probing and
manipulating MAP recognition patterns. Our findings open new avenues for precisely engineering
MT behavior in both mechanistic and therapeutic contexts.
776

Summary
Binding of stabilizing drugs to MTs alters their structure both longitudinally (through lattice
expansion) and laterally (by changing the number of PFs). In the longitudinal axis, only two
conformational states are possible: a compressed lattice (monomer rise of 4.06 nm) and an
expanded lattice (monomer rise of 4.17 nm). The energetic differences and transition barriers
between these two states are small, as even low stoichiometric ratios of a bound drug can shift
the equilibrium, and lattice expansion occurs within seconds after drug incorporation.
In contrast, multiple configurations are possible for lateral contacts, consistent with the
variable PF numbers observed among microtubules. Although the energetic differences between
MTs with different PF numbers are minor—again allowing low stoichiometric ratios of drug to
influence equilibrium—the energy barriers separating these states are considerably higher.
The conformational effects of these compounds can be finely tuned through subtle
chemical modifications, such as acylation of the C-7 secondary alcohol in paclitaxel. These
structural alterations are mirrored in the chemical properties of MTs, including their phosphatase
activity, and profoundly influence their recognition by tau and kinesin. Together, these findings
underscore the role of MT structure as a dynamic signaling platform that integrates chemical,
mechanical, and regulatory cues.
794

Materials and Methods
Proteins and chemicals.

Purified calf brain tubulin containing a mixture of isotypes (69) was obtained as
described(70) and used for biochemical, and fiber diffraction experiments. Tau-mCherry was
expressed and purified as described previously (55). Human Kif5B-eGFP (amino acids 1–905),
containing a C terminal fluorescent-tag followed by a 3C protease cleavage site and a 6 × His-
tag was expressed and purified as in (71) with some modifications. Prior to purification, cells were
re-suspended in 1:1 ratio of lysis buffer (30 mM HEPES pH 7.5, 300 mM NaCl, 0.5 mM ATP, 5%
glycerol, 20 mM imidazole, 0.5 M TCEP) supplemented with 1× Protease inhibitor cocktail and
benzonase to the final concentration of 25 units/ml. Cells were homogenized by repeated
pipetting. Cells were lysed by spinning for 45 min at 40,000 rpm in 45 Ti fixed-angle rotor
(Beckman Coulter) at 4 ºC. The supernatant was incubated with pre-equilibrated HisPUR NiNTA
agarose resin (Thermo Fisher Scientific) for 1 h in a tightly closed gravity-flow column (Thermo
Fisher Scientific) at 4 ºC by slowly rotating. Subsequently, the resin was washed once lysis buffer

and then with buffer B (30 mM HEPES pH 7.5, 300 mM NaCl, 0.5 mM ATP, 5% glycerol, 30 mM

imidazole, 0.5 M TCEP). The protein was eluted from the resin after an overnight cleavage of the

6 × His-tag with 3C HRV protease in lysis buffer at 4 ºC. The eluted protein was further purified

via size-exclusion chromatography on Superdex® 200 10/300 GL column equilibrated in

exclusion buffer (30 mM HEPES pH 7.5, 300 mM NaCl, 0.5 mM ATP, 5% glycerol, 0.5 M TCEP).

Peak fractions were analyzed via SDS-PAGE, pooled and the protein was concentrated with

Amicon Ultra-15 Centrifugal Filter tubes (Millipore). Purified proteins were aliquoted, snap-frozen

in liquid N_2, and stored at –80 ºC.

GTP and GMPCPP were from Jena Biosciences (Jena, Germany). Sodium molybdate

and Malachite green oxalate were from Sigma-Aldrich. Paclitaxel was from Alfa Aesar Chemical,

docetaxel was kindly provided by Rhône Poulenc Rorer, Aventis (Schiltigheim, France),

cabazitaxel and baccatin III were from Sigma, epothilones A, B, D, taccalonolide AJ and

ixabepilone were from MedChemExpress; laulimalide and peloruside A were provided by Victoria

University of Wellington; chitax 40, 101 y 102, 2-aminopaclitaxel, 3'N-aminopaclitaxel, flutax-1,

flutax-2, Fchitax-3, 2-m-azido-baccatin III, hexaflutax, alatax, discodermolide, zampanolide,

dactylolide, TB282, cyclostreptin, pelophen B and CW235 were synthesized as described (21,

64, 66, 72-81). FB44 and FB53 were synthesized as described (42). GS305 was synthesized as

described (10.26434/chemrxiv-2024-nwb48). The synthesis and characterization of pelophen B

is described in patent PCT/EP2014/075903

All compounds were diluted in 99.8% DMSO-d_6 (Merck) to a final concentration of 20 mM

and stored at –70 ºC.

Microtubule shear-flow alignment and X-ray fiber diffraction experiments.

MTs were assembled from purified bovine brain tubulin (100 mM) in PM buffer (80 mM K-

PIPES, 1 mM EGTA, 1 mM dithiothreitol, 0.2 mM Tris, 3 mM $MgCl_2$, pH 6.8) and either 2 mM GTP

or 0.5 mM GMPCPP, 2 mM GTP or 0.5 mM GMPCPP and the desired concentration of drug, (200

mM in the case of the static experiments), 2 mM GTP + 10 mM BeF_3^-, 2 mM GTP + 500 mM $AlCl_3$

+ 2 mM HKF_2, 2 mM GTP + 10 mM BeF_3^- + 200 mM paclitaxel or 2 mM GTP + 500 mM $AlCl_3$ + 2

mM HKF_2 + 200 mM paclitaxel. Static X-ray fiber diffraction data of microtubules were collected

in BL11-NDC-SWEET beamline of ALBA Synchrotron, Cerdanyola del Vallès (Spain) at λ = 0.827

nm, as described in (34).

Data were processed using our in-house developed software FiDAT (Fernández et al.

manuscript in preparation), dimer/monomer length (from the 4th harmonic of the first layer-line

signals) were determined as described (25, 34) while radial structural parameters (microtubule

diameter, and average PF number) were determined from the position of the J_{02} maxima

according to J_{02} = 1.045/R assuming an IPF mean distance of 5.7 nm (35).

Kinetic X-ray fiber diffraction experiments were performed at BL40XU beam line of

Spring-8, Hyogo, Japan. An aliquot of 100 μL of the suspension containing the assembled MTs at

a 100 µM concentration was collected and applied onto the shear-flow apparatus. The top end of

the apparatus was opened to enable free access to the specimen, where we set an electric pipette

(eLine, Sartorius, Gettingen, Germnay) directly connected to a wireless shutter controller

(Oppilas/L1, Pixel, China). At t = 40 s, 1 µL of DMSO stock solution containing 20 mM of stabilizers

(paclitaxel, docetaxel, chitax 40, baccatin III and laulimalide) was added by remote control of the

electric pipette to the solution to reach a final concentration 100 µM. Diffraction signals were

measured employing a 0.8 m camera length and exposure of 0.95 s and a Pilatus 200K, 475 ×

195 pixels (Rigaku, Tokyo, Japan) detector using ImageJ, ver. 1.53c (NIH, USA). The average

monomer length of the tubulin monomer was estimated from the 1 nm^{-1} layer line. Calibration of

the spacing of diffraction reflections was performed using a standard 4.97 nm signal in powder

diffraction using lead stearate. One pixel in the detector corresponded to the spatial frequency in

a reciprocal space of 0.0011 nm^{-1}. The peak position was determined by fitting each of the

obtained signal profiles to a Lorentzian function.

In silico model building and molecular dynamics simulations.

Ab initio geometry optimization and derivation of atom-centered RESP charges (82) for

docetaxel, epothilone A, zampanolide, discodermolide and alatax were accomplished by using

the density functional tight-binding method, a 6-31G(d,p) basis set, and the IEF-SCRF continuum

solvent model (83)) for water, as implemented in program Gaussian 09 (Revision D.01) (84). This

procedure has been reported earlier for other tubulin ligands (85) and for the covalent adducts of

taccalonolide AJ and zampanolide with Aspβ226 and Hisβ229, respectively (45). Bonded and

non-bonded parameters for these taxanes were obtained from the general AMBER force field

gaff2 (86). The conformational preferences of discodermolide in explicit water were studied upon

immersion of this ligand (as found in PDB entry 6SES) in a cubic box of TIP3P water molecules

and simulation at 300 K for 300 ns using molecular dynamics (MD) followed by simulating

annealing and energy minimization, as performed earlier for other drugs (42, 87).

For the ligand-bound macromolecular assemblies representing three parallel short PFs,

each consisting of two concatenated head-to-tail dimers (i.e., (α1:β1-α2:β2)/(α1':β1'-

α2':β2')/(α1":β1"-α2":β2")), use was made of PDB entries 6DPU and 6DPV (88), which depict a

stretch of an expanded or compacted 14-PF MT, respectively, and PDB entry 3JAK (89), which

corresponds to a symmetrized reconstruction of a compacted 13-PF MT. Missing residues 38–46

in each α subunit were grafted from AlphaFold model AF-P81947-F1-v4 for completeness.

Residue numbering and secondary structure assignment herein follow the α-tubulin-based

definitions (90), as is customary in the Protein Data Bank.

The refined 6DPV and 3JAK MT patches were used as input to the elNémo web server

(91) to build the corresponding anisotropic elastic network models (ENM) (92) and carry out the

normal mode analyses (NMA) employing the default values for cutoff (12 Å), force constant (1.0

kcal mol^{-1} $Å^{-2}$) and maximum displacement (amplitude <2 Å).

The interdimer space was first explored in a series of minimalist (b1:a2) complexes
originating from PDB entries 6DPU (expanded) and 6DPV (compacted) in which all Ca atoms -
except those in the more flexible and less well-defined loop regions- were positionally restrained
by means of a weak harmonic force constant (2.0 kcal mol^{-1} Å^{-2}) to preserve the gross
characteristics of each MT subtype. The GTP molecule in the N-site of α-tubulin and either GTP
or GDP in the E-site of β-tubulin, together with their partially hydrated coordinated Mg^{2+} ions, were
initially located as reported in the high-resolution X-ray crystal structures deposited with PDB
codes 4I4T and 8BDE. These systems were firstly energy refined and then simulated at 300 K for
100 ps using the *ff14SB* force field (93) for protein atoms, the TIP3P model for the few explicit
water molecules, and the generalized Born model for the bulk solvent (94), as implemented in the
pmemd.cuda_SPFP engine of AMBER 18. The resulting equilibrated systems were then
subjected to a simulated annealing procedure by gradually decreasing the temperature from 300
K to 100 K over a period of 150 ps.

The different (α1:β1-α2:β2)/(α1':β1'-α2':β2')/(α1":β1"-α2":β2") complexes in the apo and
holo states were then simulated under the same conditions for 200 ps. alatax and docetaxel were
best-fit superimposed onto the structure of bound paclitaxel, as reported earlier for similar
molecules (21). Discodermolide and epothilone B were docked in the β subunits so as to
reproduce the binding poses found in PDB entries 6SES and 7DAE, respectively. Construction of
the covalent adducts with taccalonolide AJ and zampanolide followed a previously reported
procedure (45). By following this procedure, six replicas of each bound ligand and ligand-binding
site were sampled simultaneously. The resulting equilibrated MT patches were cooled down from
300 K to 100 K over 400 ps and then energy minimized in the absence of any restraints. Next,
each refined 3´2-patch of tubulin dimers was replicated six times in PyMOL, as recently described
for similar systems (42), and the (α1:β1-α2:β2-α3:β3) stretch of the first copy was best-fit
superimposed onto the (α1":β1"-α2":β2"-α3":β3") stretch of the optimized model. Thereafter, the
(α1:β1-α2:β2-α3:β3) stretch of each remaining copy was best-fit superimposed onto the (α1":β1"-
α2":β2"-α3":β3") stretch of the preceding model. This process led quite naturally to the formation
of a tubular structure consisting of 13 or 14 straight PFs (**Figure S2**) with one drug molecule
bound in the taxane site of every β subunit. Lastly, the macromolecular ensemble was cleaned
up by removing the redundant overlaid copies to produce an all-atom model of the MT lattice,
which was subjected to a final energy refinement and sequential chain renumbering. For the 12-
and 15-PF MTs, each (α1:β1-α2:β2-α3:β3) copy was best-fit superimposed onto the
corresponding PF stretch of the harmonically deformed model obtained from the NMA (**Supp.**
Movie 11).

The resulting MT pieces representative of a full turn of laterally associated PFs with bound
paclitaxel, docetaxel, epothilone B, discodermolide, zampanolide and taccalonolide AJ have been
deposited in the publicly available ModelArchive (www.modelarchive.org) database with
accession codes ma-rkctk, ma-x9q02, ma-2embb, ma-ir5i7, ma-qcuyh, and ma-qzvr1,
respectively. The atomic model of a MT piece containing bound alatax can be inferred from that
bound to Flutax-2 (ma-ayvpr) (42). The first non-trivial normal mode calculated for the Ca trace

of the refined paclitaxel-bound 12-PF MT clearly shows the closing motion that leads to
heterotypic seam sealing (**Supp. Movie 11).**

Measurement of nucleotide hydrolysis.

Nucleotide hydrolysis by MTs was in MEDTA (100 mM potassium 2-(*N*-
morpholino)ethanesulfonic acid (K-MES), 1 mM EDTA, 3.4 M glycerol, pH 6.7) buffer containing
6 mM $MgCl_2$ and 1mM GTP. Firstly, 10 mg of lyophilized tubulin was re-suspended in 0.5 mL
MEDTA buffer, containing 0.1 mM GTP or 0.001 mM GMPCPP and without $MgCl_2$. The protein
solution was subjected to size-exclusion chromatography with a column of Sephadex G-25
medium (30 × 0.9 cm) to remove the trehalose and phosphate present in the storage buffer. Next,
aggregates were removed by centrifuging at 50.000 rpm for 10 minutes at 4 °C using a Beckman
Optima MA-XP ultracentrifuge (Beckman Coulter) equipped with a TLA 120.2 fixed-angle rotor
(Beckman-Coulter). Tubulin concentration was determined by absorption spectrophotometry
using a UV-vis spectrophotometer (Evolution 201 spectrophotometer, Thermo Scientific) with 1
cm light path quartz cuvettes. Absorbance spectra, ranging from 240–340 nm, were recorded
after preparing a 1/20 dilution with NaPi-SDS buffer. The concentration of tubulin was calculated
using the molar extinction coefficient (ε) of 107000 M^{-1} cm^{-1} at λ = 275 nm as mentioned above.
After calculating the concentration of tubulin, 6 mM $MgCl_2$ and 0.9 mM GTP or 0.099 mM
GMPCPP (to obtain a final concentration of 1 mM GTP or 0.1 mM GMPCPP) were added to the
sample.

Tubulin polymerization was induced by raising temperature to 37ºC (polymerization was
followed at λ = 355 nm in an Appliskan® plate reader (Thermo Scientific) and the phosphate
released was measured using the malachite green inorganic phosphate assay (49). Briefly, a 20
µL aliquot of the polymerized solution was diluted with 280 µL of milli-Q water and 300 µL of
malachite green solution (0.2% sodium molybdate, 0.03% malachite green oxalate, 0.05% Triton
X-100, 0.7 M hydrochloric acid) was added, mixed thoroughly, and incubated. Absorbance was
measured at λ = 650 nm and phosphate concentrations in the samples were calculated by
comparison with sodium phosphate standards. Nucleotide content in drugged assembled MTs
was quantified by centrifugation and HPLC as described in (95).

In vitro tau and kinesin- drug stabilized microtubules binding assay.
The *in vitro* binding of Kif5B1-950-eGFP and tau441-mCherry to drug stabilized MTs was
measured using TIRF microscopy as described in (96) by replacing paclitaxel with the desired
drug. TIRF microscopy experiments were performed on an inverted widefield microscope
Nikon-Ti2 E, equipped with a motorised XY-stage, a perfect focus system, Apo TIRF 60× oil NA
1.49 objective and PRIME BSY (Teledyne Photometrics) camera. MTs were visualized using
Interference Reflection microscopy (IRM) and fluorescently labelled proteins were visualized
sequentially by switching between microscope filter cubes for GFP and mCherry channels. The

microscope was controlled using NIS Elements software (Nikon). All experiments were conducted
at RT.

Microscopy chambers were prepared from two sandwiched silanized glass coverslips (22
× 22 mm and 18 × 18 mm) attached through parafilm strips (heated for 15–20 s at 60 °C and
gently pressed together) to form ~2.5 mm wide parallel flow channels. Prior to the chamber
assembly, the coverslips were washed in 3 M KOH, cleaned using Zepto plasma cleaner (Diener
electronic) and silanized with hexamethyldisilazane. Flow channels were first incubated with 40
µg mL^{-1} anti-biotin antibodies (Sigma, B3640) in PBS for 10 min, followed by incubation with 1%
Pluronic F127 (Sigma Aldrich, P2443) in PBS for at least 1 hour. Then, F127 was washed with
BRB80 (80 mM PIPES, 1 mM EGTA, 1 mM MgCl$_2$, pH 6.9).

The MTs employed were assembled from porcine brain tubulin isolated using the
high-molarity PIPES procedure (97). MTs were assembled using 2% biotin-labelled tubulin
(Cytoskeleton Inc., T333P). Drug-stabilized, pre-assembled MTs (polymerized, stored and
imaged in presence of desired drug) were polymerized from 4 mg mL^{-1} 2%-biotinylated tubulin
for 30 min at 37 °C in BRB80 supplemented with 4 mM MgCl$_2$, 40 µM of the desired drug using
5% DMSO, and 1 mM GTP (Jena Bioscience, NU-1012). MTs were centrifuged for 30 min at
18,000×g in a Microfuge 18 Centrifuge (Beckman Coulter). The pellet was re-suspended and kept
in BRB80 supplemented with 10 µM of the desired drug. GMPCPP stabilized MTs (GMPCPP
polymerized) were assembled from 4 mg mL^{-1} 2% biotinylated tubulin for 2 h at 37 °C in BRB80
supplemented with 1 mM MgCl$_2$ and 1mM GMPCPP (Jena Bioscience, NU-405). Polymerized
MTs were centrifuged for 30 min at 18,000xg in a Microfuge 18 Centrifuge (Beckman Coulter)
and pellets were re-suspended and kept in BRB80.

Stabilized MTs were flushed into the channel and incubated for 10–20 seconds to allow
for surface attachment. Unbound MTs were removed by washing with BRB80 supplemented with
10 µM of the desired drug. Prior the experiment, the solution was exchanged by motility buffer
(BRB80 containing 10 mM DTT, 20 mM D-glucose, 0.1% Tween-20, 0.5 mg/mL casein, 1 mM
Mg-ATP, 0.02 mg/mL catalase, 0.22 mg/mL glucose oxidase, 10 µM drug). Subsequently, a
solution containing either 10.8 nM Kif5B-eGFP or 5/10/40 nM tau-mCherry in MB was introduced
into the chamber.

To assess Kif5B-eGFP motility along MTs, an IRM image (50 ms exposure) was acquired
followed by a 1 min video using 488 nm laser excitation (20% laser intensity, 300 ms exposure)
with no delay. Three to four videos were recorded from different fields within the same channel
and at least 2 channels were measured for each experimental condition. The same experiment
was done in 2 to 3 different days giving an n between 12 and 24.

To monitor tau-mCherry binding to MTs, 4 min videos were acquired every 7 sec. Two
imaging channels were recorded simultaneously, alternating between IRM (50 ms exposure) and
561 nm field (30% intensity, 200 ms exposure). Depending on the drug used, firstly 5/10 nM
tau-mCherry was injected immediately after the first frame was acquired. Similarly, a second/third
video of the same area was recorded adding an additional 10 and 40 nM tau-mCherry.

1002

Image analysis.

       For representative figures, all data were collected from at least two independent trials. Unless otherwise stated, all data were analysed manually using Fiji (ImageJ) (98); graphs and statistical analyses were created and performed using GraphPad Prism v.8.0.1. Graphs represent mean data, and the error bars represent the standard errors of the mean (SEM).

       Background fluorescence was subtracted from all intensity measurements. For each condition, analyses were performed on 12 randomly selected, in-focus MTs per channel, being identified with IRM.

       For kinesin motility analysis, MTs were selected in the IRM channel by drawing segmented lines of 5 pixels in width. Kymographs were generated using the *KymographBuilder* plugin of Fiji. Individual motor traces were manually selected as straight lines (1 pixel thick) on the kymographs. From these traces, run length (x-axis), interaction time (y-axis), and velocity (calculated as the ratio of both) were determined using the Multiple Velocity Measurement Tool macro that applies to all ROIs in the ROI Manager of Fiji. Finally, landing rate was assessed by quantifying the number of kinesins bound along each MT and normalizing this value to the total MT length (expressed in mm) and time.

       To quantify the fraction of the MT surface covered by tau envelopes, a segmented line with a fixed width of 5 px (0.36 mm) was manually traced along either the envelope-covered regions or the full length of individual MTs. The total length of all envelope segments was then divided by the corresponding MT length to yield the percentage of coverage. This analysis was conducted at multiple time frames: four time points (12 s, 1, 2 and 4 min) in the first video recorded under 5/10 nM tau-mCherry, and three time points (12 s, 2 and 4 min) for the subsequent conditions. To compare the amount of tau bound per micron of MT across different structural conditions, a segmented line (5 px wide) was drawn along the entire length of each MT. The integrated fluorescence intensity (IntDen) was measured, and this value was normalized to the background and divided by the corresponding MT length (in mm). This analysis was performed at three time points (12 s, 2 and 4 min) in the sequential videos.

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1283   *Supplementary Information.*

1284

Figure S1. Helix H7 as a transducer of conformational changes between the taxane-
binding site (orange oval), the exchangeable nucleotide site (E site, yellow oval) and the
M-loop (an alpha-helix when PFs are associated laterally). Ribbon representation of the
interdimer interface from a compressed PF (β1, light pink and α2, dark pink) with bound
discodermolide (C atoms in orange) displayed as a representative taxane site-binding ligand. The
C atoms of the GDP and GTP nucleotides are colored yellow and salmon, respectively. Mg^{2+} ions
are displayed as green spheres and relevant residues mentioned in the text have been labeled.
1292

Figure S2. Schematic describing the procedure followed for constructing a full turn of a 13-PF compacted MT fragment with one discodermolide (DDM) molecule bound to the β subunit of each tubulin dimer (https://modelarchive.org/doi/10.5452/ma-ir5i7). Briefly, the initial template was provided by a short MT patch consisting of three laterally associated PFs, each made up of two head-to-tail concatenated tubulin dimers, as deposited in the Protein Data Bank with id. 3JAK. The interdimer interfaces in this cryo-EM structure were optimized with the aid of information provided by the high-resolution X-ray crystal structures 8BDE and 8BDF (for the GDP and GTP nucleotides, Mg^{2+} ions and hydration shell waters) and 5LXT (for the ligand bound at the taxane site in β-tubulin) together with energy refinement using the AMBER force field. The resulting optimized patch was replicated six times in PyMOL. The (α1:β1-α2:β2) stretch of the first copy was then best-fit superimposed onto the (α1":β1"-α2":β2") stretch of the original refined model. Thereafter, the (α1:β1-α2:β2) stretch of each remaining copy was best-fit superimposed onto the (α1":β1"-α2":β2") stretch of the preceding model. This process led quite naturally to formation of a tubular structure consisting of 13 straight PFs with one DDM molecule lodged in the taxane site of every β subunit. Lastly, the macromolecular ensemble was (i) cleaned up by removing the redundant subunit copies used for the superposition and (ii) energy refined in the AMBER force field. A similar procedure was followed to obtain the other complexes reported in this paper, as described in the corresponding entries of the ModelArchive repository. For epothilone B and zampanolide, additional use was made of normal mode analysis to create the 12- and 15-PF MT structures (ModelArchive entries ma-2embb and ma-qcuyh, respectively), as reported previously for paclitaxel (ma-rkctk).

Supp. Movie 1: Representative time-resolved fiber diffraction images. Sequence of images showing fiber diffraction patterns of Apo-MTs and their structural response to the addition of an 2x excess of drug at time = 40 s. (**A** paclitaxel, **B** docetaxel, **C** baccatin III, **D** laulimalide)

Supp. Movie 2: Conformational changes observed by calculating the first non-trivial normal mode for a MT patch consisting of three laterally associated dimers of dimers (PDB id. 6DPV) using the elNemo web server and the default amplitude value. The three views correspond to three orthologous viewpoints. Note that (i) greater amplitudes can be achieved if a bound ligand further stretches the structure along the normal mode and locks the ensemble in this state until ligand

1327 dissociation takes place, and (ii) a decrease in lateral curvature will result in an increase in the
1328 number of component PFs and vice versa.
1329
1330 **Supp. Movie 3. Representative video of Kif5B-eGFP movement along drug-stabilized MTs.**
1331 1-minute video of 10.8 nM Kif5B-eGFP using a 488 nm laser (20% laser intensity, 300 ms
1332 exposure) was acquired with no delay (20 fps).
1333
1334 **Supp. Movie 4. Tau binding to zampanolide-stabilized MTs**. 4 min videos of 5 nM tau-mCherry
1335 using a 561 nm laser (30% intensity, 200 ms exposure) were acquired every 7 s.
1336
1337 **Supp. Movie 5. Tau binding to discodermolide-stabilized MTs**. 4 min videos of 5 nM
1338 tau-mCherry using a 561 nm laser (30% intensity, 200 ms exposure) were acquired every 7 s.
1339
1340 **Supp. Movie 6. Tau binding to laulimalide-stabilized MTs**. 4 min videos of 5 nM tau-mCherry
1341 using a 561 nm laser (30% intensity, 200 ms exposure) were acquired every 7 s.
1342
1343 **Supp. Movie 7. Tau binding to epothilone B-stabilized MTs**. Sequential 4 min videos of (**A**)
1344 10 nM and (**B**) 40 nM tau-mCherry using a 561 nm laser (30% intensity, 200 ms exposure) were
1345 acquired every 7 s.
1346
1347 **Supp. Movie 8. Tau binding to docetaxel-stabilized MTs**. Sequential 4 min videos of (**A**) 10
1348 nM and (**B**) 40 nM tau-mCherry using a 561 nm laser (30% intensity, 200 ms exposure) were
1349 acquired every 7 s.
1350
1351 **Supp. Movie 9. Tau binding to peloruside A-stabilized MTs**. Sequential 4 min videos of (**A**) 5
1352 nM, (**B**)10 nM and (**C**) 40 nM tau-mCherry using a 561 nm laser (30% intensity, 200 ms exposure)
1353 were acquired every 7 s.
1354
1355 **Supp. Movie 10. tau binding to pelophen B-stabilized MTs**. Sequential 4 min videos of (**A**) 10
1356 nM and (**B**) 40 nM tau-mCherry using a 561 nm laser (30% intensity, 200 ms exposure) were
1357 acquired every 7 s.
1358
1359 **Supp. Movie 11**: Conformational changes observed by calculating the first non-trivial normal
1360 mode for a short full-circle MT consisting of twelve laterally associated PFs using the elNemo web
1361 server and twice the default amplitude value. The three views correspond to three orthologous
1362 viewpoints. Note that the motion shown will lead to sealing of the PF gap between the first and
1363 the twelfth PF.