

1 **A short, robust brain activation control task optimised for**  
2 **pharmacological fMRI studies.**

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## 23 **Abstract**

24 Functional magnetic resonance imaging (fMRI) is a popular method for examining  
25 pharmacological effects on the brain; however the BOLD response is an indirect  
26 measure of neural activity, and as such is vulnerable to confounding effects of  
27 pharmacological probes. Controlling for such non-specific effects in pharmacological  
28 fMRI studies is therefore an important consideration. We have developed two variants  
29 of a standardized control task that are short (5 minutes duration) simple (for both the  
30 subject and experimenter), widely applicable, and yield a number of readouts in a  
31 spatially diverse set of brain networks. The tasks consist of four functionally discreet  
32 three-second trial types (plus additional null trials) and contain visual, auditory, motor  
33 and cognitive (eye-movements, and working memory tasks in the two task variants)  
34 stimuli. Performance of the tasks was assessed in a group of 15 subjects scanned on two  
35 separate occasions, with test-retest reliability explicitly assessed using intra-class  
36 correlation coefficients. Both tasks produced robust patterns of brain activation in the  
37 expected brain regions, and reliability coefficients for the tasks were generally high, with  
38 four out of eight task conditions rated as 'excellent', and only one out of eight rated as  
39 'poor'. Voxel-wise reliability measures also showed good spatial concordances with the  
40 brain activation results. Either of the two task variants would be suitable for use as a  
41 control task in future pharmacological fMRI studies or for any situation where a short,  
42 reliable, basic task paradigm is required. Stimulus code is available online for re-use by  
43 the scientific community.

## 44 Introduction

45

46 Functional Magnetic Resonance Imaging (fMRI) is currently one of the major standard  
47 methods in cognitive neuroscience research. FMRI provides reasonably high spatial and  
48 temporal resolution data, is flexible enough to accommodate a wide variety of  
49 experimental designs, and exposure to magnetic fields presents no danger to most  
50 subjects (Logothetis, 2008; Soares *et al*, 2016). FMRI can also be used as an index of  
51 pharmacological effects; drugs or hormones can be administered before or during a  
52 scanning session, and the results compared with a baseline or placebo session (e.g.  
53 Carhart-Harris *et al*, 2014; Comninos *et al*, 2017; Kaelen *et al*, 2016; Upadhyay *et al*,  
54 2011). Pharmacological-fMRI studies may be used in the drug discovery process  
55 (Matthews *et al*, 2011; Wise and Tracey, 2006), in the characterization of the effects of  
56 commonly-prescribed drugs (Maron *et al*, 2016), or in the exploration of disorders such  
57 as addiction (Quelch *et al*, 2017).

58 Conducting pharmacological-fMRI investigations presents many of the same challenges  
59 as standard fMRI, but also has some unique issues. One fundamental concern is related  
60 to the fact that (most commonly) fMRI studies use the BOLD (Blood-Oxygen-Level-  
61 Dependent) signal as the primary end-point. This is a contrast produced by local changes  
62 in the ratio of oxygenated and de-oxygenated hemoglobin (Buxton *et al*, 1998; Friston *et al*,  
63 2000), and is usually regarded as a proxy measure of neural activity. However, the  
64 relationship between neural activity and this vascular response (neurovascular coupling)  
65 is complex and relies on a number of cellular and metabolic processes (Logothetis *et al*,  
66 2001). Use of a pharmacological agent combined with fMRI means that any differences  
67 observed in the BOLD response may be a combination of direct neural effects of the  
68 drug (usually the effects of interest), and indirect effects of the drug (e.g. on  
69 neurovascular coupling, or global, systemic effects on blood-pressure, cerebral blood  
70 flow, heart-rate, etc.; usually regarded as confounding effects). One example is caffeine  
71 which has direct neural effects on adenosine A<sub>1</sub> and A<sub>2a</sub> receptors, but is also a powerful  
72 cerebral vasoconstrictor (Diukova *et al*, 2012). Separating the neural and vascular effects

73 of even such a selective and widely-studied drug as caffeine is therefore a considerable  
74 challenge. For detailed reviews of these issues see Bourke and Wall (2015), and Iannetti  
75 and Wise (2007).

76 One method of mitigating this problem is the use of an independent control task  
77 paradigm as part of a pharmacological fMRI scanning session (Iannetti and Wise, 2007).  
78 For example, Murphy *et al* (2009) used a visual control task in their study of the effect of  
79 citalopram on amygdala responses to emotional faces. In this case the lack of effect of  
80 the drug on the visual control task suggests that the effects seen in the main task are  
81 unlikely to be due to effects on neurovascular coupling, or other global/systemic effects.  
82 However, the use of a single (visual) control task, which gives activation in a subscribed  
83 region of the brain (the occipital lobe) is suboptimal as indirect effects on neurovascular  
84 coupling may still vary across the brain. Comninos *et al* (2017) used a much more  
85 elaborate control task (based on Pinel *et al*, 2007) in their recent study on the sex  
86 hormone kisspeptin. This task involved ten trial conditions which gave results in five  
87 separate functional domains (visual, auditory, language, motor, and cognitive), and in a  
88 much wider spatial distribution across the brain. This task involved relatively complex  
89 instructions for the subjects, and also included some culturally-specific language stimuli,  
90 which somewhat limits its broad applicability.

91 An ideal task for the control of pharmacological fMRI studies should have the following  
92 characteristics. First, it should be short in duration as it generally has to be included as  
93 part of a broader set of functional task paradigms, anatomical scans, and perhaps other  
94 MRI measures (resting-state fMRI, perfusion measures, spectroscopy etc.). Second, it  
95 should be simple, both for the subject to perform and for the experimenter to run and  
96 analyse. It should require no complex instructions, and depend upon only standard  
97 equipment (standard computer hardware/software, audiovisual systems, and simple  
98 response devices). Third, it should contain a number of different trial types, which  
99 produce activation in different brain networks, in as wide a spatial distribution across  
100 the brain as possible. This helps to rule out effects on neurovascular coupling which may

101 differ in spatially remote brain regions. Fourth, it should be general-purpose; applicable  
102 to a wide range of different pharmacological fMRI studies. Fifth, it should be reliable; it  
103 should produce robust results within a single-session, and produce reliable results  
104 across multiple sessions. This last point is of particular importance, as use of an  
105 unreliable control task would constitute an additional confound, however no previous  
106 pharmacological fMRI study has explicitly assessed the reliability of its control task.  
107 Indeed reliability is relatively seldom formally assessed in fMRI studies (Plichta *et al*,  
108 2012).

109 We have developed two variants of a task paradigm that meet the above mentioned  
110 criteria, and are furthermore programmed in an open-source software environment  
111 (PsychoPy; Peirce, 2007, 2008). One variant consists of visual, auditory, motor, and eye-  
112 movement trials. The other substitutes a brief working-memory task for the eye-  
113 movement trials, but is otherwise identical. Both are short (5 minutes in duration),  
114 simple (requiring only standard audiovisual equipment, and a single-button response  
115 box), and both produce four robust, distinct, and specific patterns of brain activation in  
116 widely-distributed brain regions. The reliability of the task variants across two scanning  
117 sessions has been explicitly assessed using a combination of voxel-wise and Region of  
118 Interest (ROI) based approaches.

## 119 **Methods**

### 120 *Subjects*

121 15 healthy subjects (6 males, 9 females) from ages 21-48 (mean age = 30) were scanned  
122 on two separate occasions with the average re-test interval being two weeks. All  
123 participants were fully briefed and provided informed consent.

### 124 *Task Design and Procedure*

125 The tasks were programmed in PsychoPy (Peirce, 2007, 2008); a free, open-source,  
126 cross-platform Python library optimized for experimental design. The task consisted of 5  
127 discreet trial types: auditory, visual, motor, cognitive and null trials, each lasting exactly  
128 three seconds. A small red, square fixation point was present throughout each task  
129 (except in one trial type, as noted below) at the centre of the screen. Auditory trials  
130 presented six pure tones for 0.5s each, at frequencies of 261.63Hz, 293.66Hz, 329.63Hz,  
131 349.23Hz, 440Hz, and 493.88Hz (corresponding to the musical pitches C<sub>4</sub>, D<sub>4</sub>, E<sub>4</sub>, F<sub>4</sub>, A<sub>4</sub>,  
132 and B<sub>4</sub>, respectively). The order of the six tones was randomly determined on each trial.  
133 Visual trials consisted of a centrally-presented sine-wave grating subtending  
134 approximately 10° of visual angle and with a spatial frequency of 1.2 cycles/degree. The  
135 grating drifted laterally at a rate of 6 cycles per second, and the direction of drift  
136 reversed every 0.5s. Motor trials consisted of three presentations of a small image of a  
137 button, presented just above the centre of the screen, for 1s each. This was a cue for  
138 subjects to press the response box key, and the button image disappeared after each  
139 response was made. The 'cognitive' trial differed in the two variations of the task. In the  
140 eye-movement variant, the fixation point moved to six different locations corresponding  
141 to the compass locations North-East, East, South-East, North-West, West, and South-  
142 West. These points were mapped on a circle with a radius of approximately 8.75° of  
143 visual angle. Each location was maintained for 0.5s, and all six were presented (in a  
144 random order) in each three second trial. In the working-memory variant of the  
145 experiment, the cognitive trial consisted of a brief working memory task. This involved  
146 the presentation of two letter strings (containing four letters each), followed by a single

147 letter. The subject's task was to indicate whether the final, single letter was present in  
148 the first letter string. If the final letter was present in the first letter string, they were  
149 instructed to push the response button. If the final letter was not present in the first  
150 letter string they were instructed to make no response. For half the working memory  
151 trials the final letter was present in the first string, and for half it was not present.  
152 Finally, in the null trials the fixation point was maintained for three seconds, with no  
153 other stimuli presented.

154 The two task variants were identical, except for the inclusion of eye-movement trials in  
155 one, and working-memory trials in the other. Each task consisted of 100 trials (20 of  
156 each of the four active conditions, plus 20 null trials) presented in a standardized  
157 pseudo-random order. Separate versions of the two tasks reversed the trial order, and  
158 the order of presentation of these versions was counter-balanced across subjects and  
159 scans. The order of presentation of the two task variants in the scan sessions was also  
160 systematically varied across subjects and scans. The task durations were exactly five  
161 minutes (100 trials of 3s duration) plus a 10 second buffer period at the end.

162 Prior to each scan session, subjects were shown a demonstration version of each variant  
163 of the task, and instructed how to perform them. During the scanning session, visual  
164 stimuli were projected through a wave guide in the rear wall of the scanner room onto a  
165 screen mounted in the rear of the scanner bore. This was viewed in a mirror mounted to  
166 the head coil. Participants received auditory stimuli and instructions via MRI-compatible  
167 headphones, and responded using a one-button response box held in their right hand.  
168 Responses were recorded using PsychoPy's data-logging routines.

#### 169 *MRI data acquisition and analysis*

170 Data were acquired on a Siemens 3T Magnetom Trio MRI scanner (Siemens Healthcare,  
171 Erlangen, Germany), equipped with a 32-channel phased-array head coil. A high-  
172 resolution T1-weighted image was acquired at the beginning of each scan using a  
173 magnetization prepared rapid gradient echo (MPRAGE) sequence with parameters from  
174 the Alzheimer's Disease Research Network (ADNI; 160 slices x 240 x 256, TR = 2300 ms,

175 TE = 2.98 ms, flip angle = 9°, 1 mm isotropic voxels, bandwidth = 240Hz/pixel, parallel  
176 imaging factor = 2; Jack *et al*, 2008). Functional data collection used an echo-planar  
177 imaging (EPI) sequence for BOLD contrast with 36 axial slices, aligned with the AC-PC  
178 axis (TR = 2000ms, TE = 31ms flip angle = 80°, 3mm isotropic voxels, parallel imaging  
179 factor = 2, bandwidth = 2298Hz/pixel). Each functional scan lasted five minutes and ten  
180 seconds and consisted of 155 volumes.

181 Analysis was completed with FSL version 5.0.4 (FMRIB's software Library; Oxford Centre  
182 for Functional Magnetic Resonance Imaging of the Brain; [www.fmrib.ox.ac.uk/fsl/](http://www.fmrib.ox.ac.uk/fsl/)).  
183 Anatomical Images were initially skull-stripped using BET (Brain Extraction Tool;  
184 included in FSL). Images were pre-processed with standard parameters (head-motion  
185 correction, 100 s temporal filtering, 6 mm spatial smoothing, co-registration to a  
186 standard template). First-level analysis used a General Linear Model (GLM) approach  
187 with the four active conditions modelled as separate regressors and the null trials  
188 implicitly modelled as the baseline. Also included were the first temporal derivatives of  
189 each time-series and head-motion parameters as regressors of no interest. Group level  
190 analyses computed a simple mean across all subjects and both scan sessions using FSL's  
191 FLAME-1 model and a statistical threshold of  $Z=3.1$ ,  $p<0.05$  (cluster-corrected).  
192 Contrasts were defined to isolate the response to each trial type relative to the null  
193 trials (baseline sections of the time-series). Two separate sets of analyses were  
194 conducted, for data from the two task variants.

195 Additional analyses used Intra-Class Correlation (ICC) coefficients to assess the reliability  
196 of responses across the two scanning sessions. This was performed in two ways; using  
197 an ROI-based approach, and by generating statistical maps of ICC values in a voxel-wise  
198 manner. For the ROI analysis, five regions were defined based on expected locations of  
199 brain activation in the tasks: primary auditory cortex in the superior temporal lobe  
200 (bilateral; auditory trials), primary visual cortex in the calcarine sulcus (bilateral; visual  
201 trials), left-hemisphere motor cortex (motor trials), the Frontal Eye Fields (FEF; bilateral;  
202 eye-movement trials), and the Dorso-Lateral Pre-Frontal Cortex (DLPFC; bilateral;



203 working memory trials). ROIs were defined as 5mm-radius spheres, and positioning  
204 coordinates were determined using guidance from relevant meta-analytic terms on  
205 Neurosynth (<http://neurosynth.org/>). The ROI definition was therefore performed  
206 completely independently from the main experimental data. Activation amplitude data  
207 was extracted from these ROIs for all subjects/scans and ICC(3,1) statistics were  
208 calculated using SPSS (IBM Corp; Armonk, NY).

209 The ICC statistical maps were produced using custom Python code and produced  
210 voxelwise images of ICC(3,1) statistics. For the purposes of thresholding the results, the  
211 ICC values were then transformed into standardized values (Z scores) using the method  
212 of Fisher (1915). These images were then thresholded using the same statistical  
213 criterion used for the group level BOLD activation analyses;  $Z > 3.1$ ,  $p < 0.05$  (cluster-  
214 corrected for multiple comparisons). These thresholded images were then used to mask  
215 the original ICC voxelwise images, to finally produce a robustly thresholded image,  
216 which also retains the original, more intuitive, ICC values.

## 217 **Results**

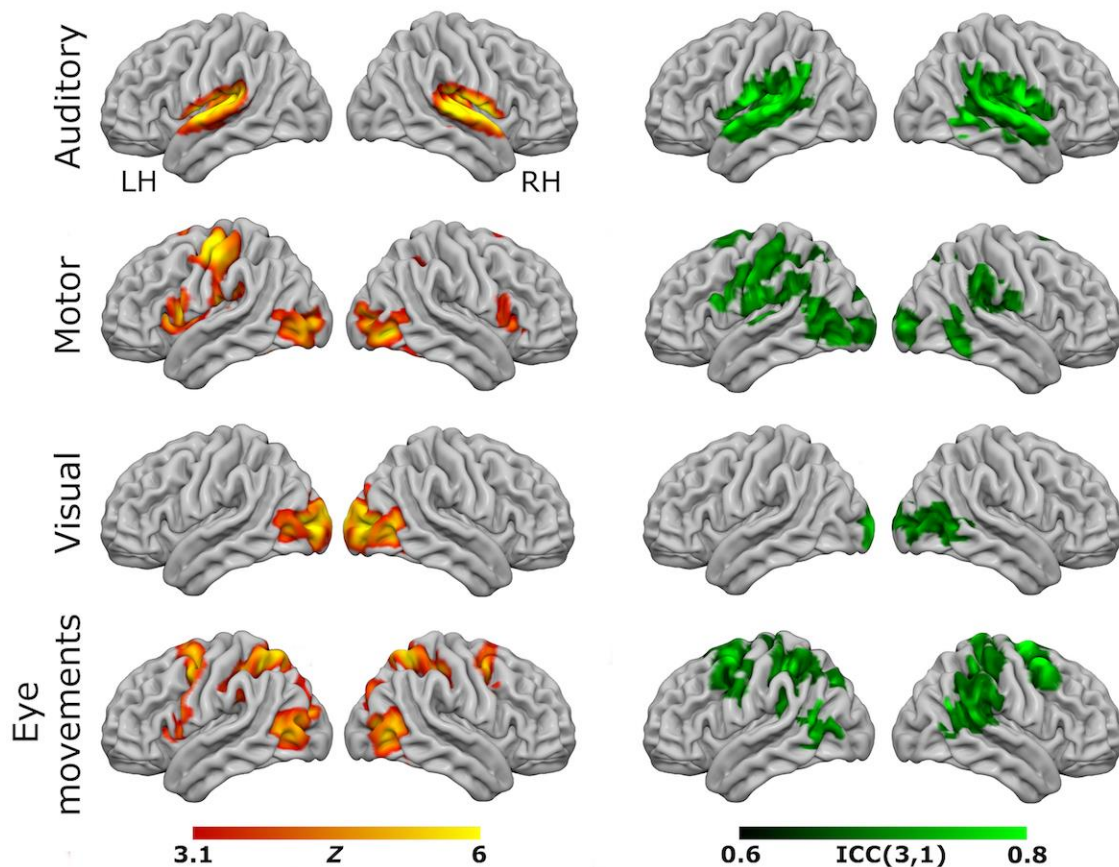
### 218 *Behavioural performance*

219 Subjects' behaviour was recorded and analysed to verify compliance with the task  
220 demands. An average accuracy rate of 93% was achieved within the working memory  
221 task. 94% and 97% accuracy was achieved for the motor task within the eye movement  
222 variant and working memory variant, respectively. All subjects performed the tasks  
223 satisfactorily.

### 224 *Group-level task activation*

225 All tasks performed as expected and produced robust patterns of brain activity in  
226 regions previously shown to be activated by similar tasks. Performance of auditory,  
227 visual, and motor components of the tasks was consistent across both task variants (see  
228 figures 1a and 2a). Auditory trials produced strong bilateral activation within the  
229 superior temporal regions, consistent with primary auditory cortex (Robson *et al*, 1998).  
230 Visual trials produced activity in posterior calcarine sulcus and the occipital pole  
231 (primary visual cortex), and in the lateral visual region V5/MT+ (Smith *et al*, 2006; Wall  
232 *et al*, 2008). Motor trials produced activity in the left-hemisphere post-central sulcus,  
233 consistent with the known location of the hand representation in primary motor cortex  
234 (Lotze *et al*, 2000).

235 In the eye-movement variant of the experiment, the eye-movement task produced  
236 activation in the Frontal Eye Fields (FEF), alongside activity within V5/MT+, the anterior  
237 portion of the calcarine sulcus/primary visual regions, and the intraparietal sulcus (see  
238 figure 1). This is generally consistent with previous reports of brain activity associated  
239 with eye-movement tasks. In the working-memory variant of the experiment, the  
240 working memory trials produced a highly robust activation pattern corresponding  
241 closely to that shown in conventional working memory tasks, such as the N-back (Owen  
242 *et al*, 2005). These regions included bilateral DLPFC, intraparietal sulcus, superior  
243 parietal lobule, dorsal anterior cingulate and the temporo-parietal junction (see figure  
244 2).



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Figure 1. Results from the eye-movement variant of the task paradigm. Results of group-level analyses represented on a cortical surface rendering of a standard anatomical image (MNI152). Left column: Active brain regions for each contrast (mean of both scanning sessions) with functional maps thresholded at  $Z > 3.1$ ,  $p < 0.05$  (cluster-corrected). Right column: Results of the reliability analysis comparing session 1 to session 2; Intra-class correlation (3,1) maps, masked with a Z-transformed, thresholded ( $Z > 3.1$ ,  $p < 0.05$ ; cluster-corrected) version in order to produce a robustly-thresholded image, while retaining the original ICC values (see methods for full details). Rows 1-4 are auditory, motor, visual and eye-movement trials.

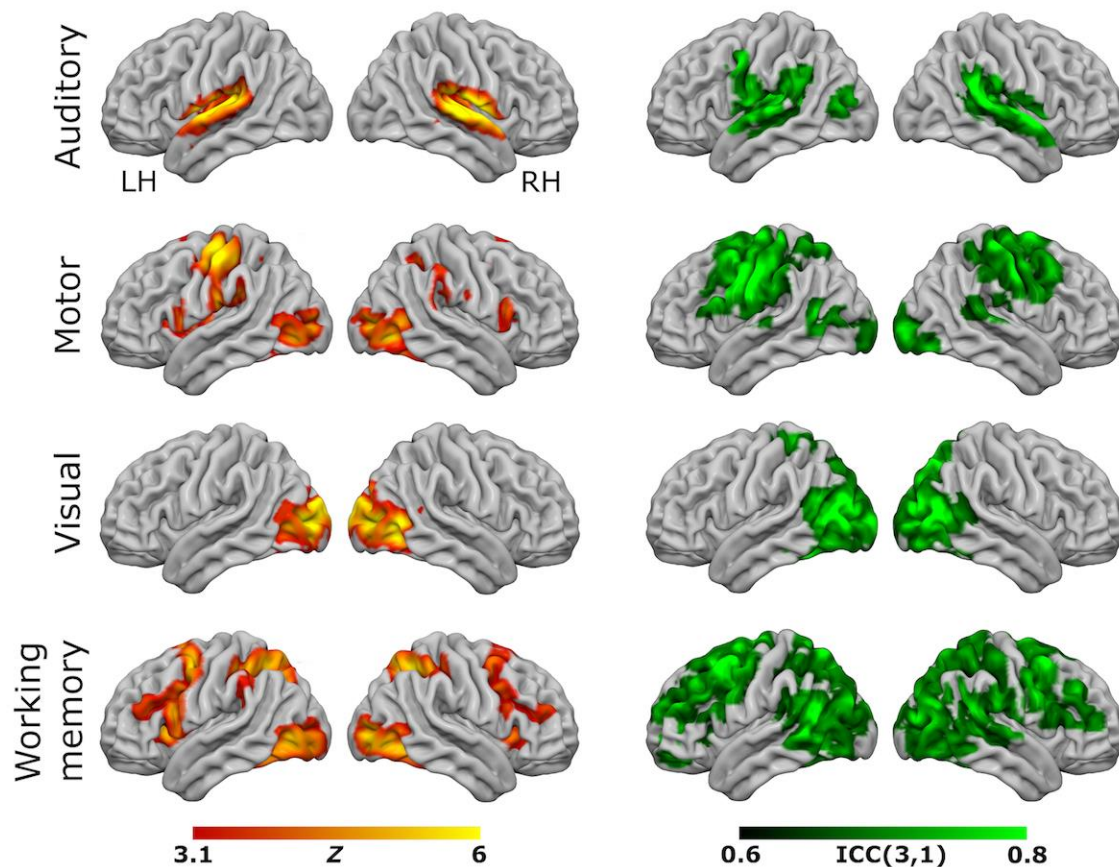
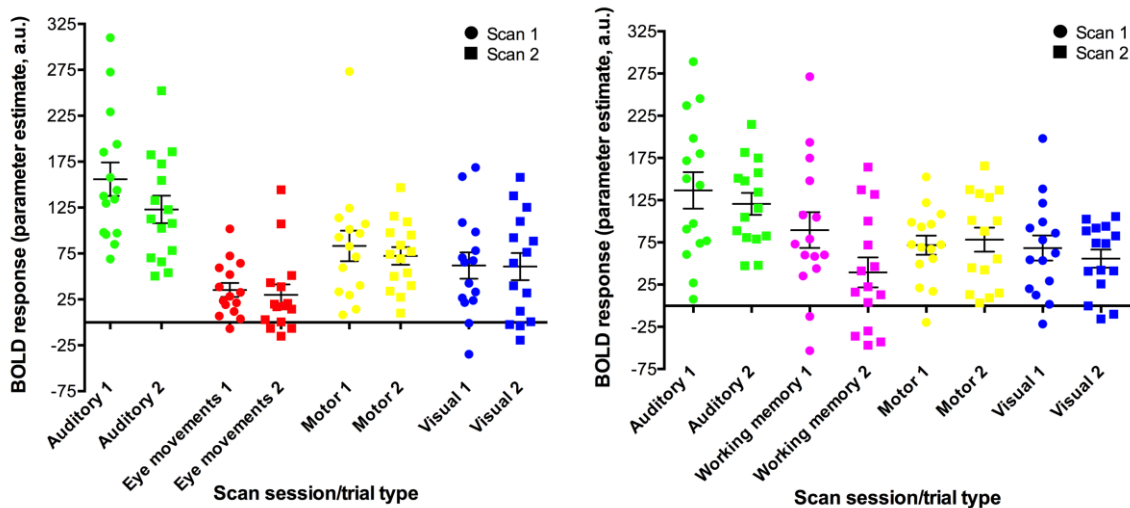


Figure 2. Results from the working-memory variant of the task paradigm. Results of group-level analyses represented on a cortical surface rendering of a standard anatomical image (MNI152). Left column: Active brain regions for each contrast (mean of both scanning sessions) with functional maps thresholded at  $Z > 3.1$ ,  $p < 0.05$  (cluster-corrected). Right column: Results of the reliability analysis comparing session 1 to session 2; Intra-class correlation (3,1) maps, masked with a Z-transformed, thresholded ( $Z > 3.1$ ,  $p < 0.05$ ; cluster-corrected) version in order to produce a robustly-thresholded image, while retaining the original ICC values (see methods for full details). Rows 1-4 are auditory, motor, visual and working memory trials.

Parameter estimate data were extracted from each contrast using a set of five ROIs: primary auditory cortex (auditory trials), frontal eye-fields (eye-movement trials), left-

271 hemisphere primary motor cortex (motor trials), primary visual cortex (visual trials), and  
272 dorsolateral-prefrontal cortex (working memory trials). These data are plotted for each  
273 condition and scan session in figure 3. Statistical analysis of these data used paired *t*-  
274 tests to compare data from each contrast across the two scanning sessions, and a  
275 Bonferroni-corrected alpha value of  $p < 0.00625$  (corrected for 8 comparisons). None of  
276 the comparisons showed significant results except for auditory trials, in the eye-  
277 movement variant;  $t(14) = 3.341$ ,  $p = 0.00485$ .



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279 Figure 3. ROI data for each task condition within the two task variants (left panel  
280 = eye-movement variant, right panel = working-memory variant). Units are  
281 parameter estimates resulting from each of the four contrasts in each GLM  
282 analysis, relative to baseline (null trials) and are arbitrary units. ROIs are primary  
283 auditory cortex (auditory trials; green), frontal eye-fields (eye-movement trials;  
284 red), left-hemisphere primary motor cortex (motor trials; yellow), primary visual  
285 cortex (visual trials; blue), and dorsolateral-prefrontal cortex (working memory  
286 trials; pink). See supplementary figure 3 for images of the ROIs.

287

288 *Reliability analyses*

289 To assess voxel level reliability, intra-class correlation (ICC(3,1)) maps were created for  
290 each task (figures 1 and 2; right columns). These show a spatial distribution very similar  
291 to the activation maps, with peak reliability estimates generally corresponding to the  
292 location of peak task-related activation. Reliability estimates in the working-memory  
293 variant of the task were generally higher and more widespread than in the eye-  
294 movement variant. For additional visualizations of the spatial correspondence between  
295 the activation maps and the ICC results, see supplementary figures 1 and 2.

296 In the ROI analysis, 4/8 ROIs featured ICC values of 0.75 or above, which is classed as  
297 'excellent' under Cicchetti's (1994) scheme for interpretation of ICC results. A further  
298 three ROIs had values in the range 0.4-0.59 which is classed as 'fair' reliability. Only one  
299 was < 0.4, and thus classed as 'poor'. The auditory task featured the most robust  
300 reliability, with values of 0.849 in the eye-movement variant and 0.840 in the working-  
301 memory variant. The DLPFC ROI showed strong reliability of 0.589 for the working-  
302 memory task, and the FEF ROI had a similar score of 0.524 for the eye-movement task.  
303 Reliability within the primary visual cortex ROI was relatively low in the eye-movement  
304 variant of the task (0.466), however this ROI was highly reliable (0.765) in the working-  
305 memory variant. A similar dissociation was seen in the left motor cortex ROI with  
306 relatively poor reliability seen in the eye-movement variant (0.258) but much higher  
307 reliability (0.778) in the working-memory variant (Table 1).

308 Unthresholded statistical maps resulting from all the group-level analyses (brain  
309 activation maps, and the voxel-wise ICC maps) are available to view at:  
310 <https://neurovault.org/collections/3264/>

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Eye-movement variant		Working memory variant	
Task condition	ICC (3,1): Scan 1 vs. Scan 2	Task condition	ICC (3,1): Scan 1 vs. Scan 2
Auditory	<b>0.849</b>	Auditory	<b>0.84</b>
Visual	<i>0.434</i>	Visual	<b>0.765</b>
Motor	0.258	Motor	<b>0.778</b>
Eye-movement	<i>0.524</i>	Working memory	<i>0.589</i>

313 Table 1. ICC(3,1) values for the different trial conditions, in both variants of the  
314 experiment. Values in bold are classed as having ‘excellent’ reliability, those in  
315 italics are classed as having ‘fair’ reliability (Cicchetti, 1994).

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## 318 Discussion

319 We have developed and successfully validated two variants of a novel fMRI control task  
320 and demonstrated that they show high test-retest reliability. These tasks are short (five  
321 minutes duration), relatively simple for both the experimenter and subject (they require  
322 only standard audio-visual presentation equipment and a one-button response box),  
323 highly robust in terms of the amplitude of brain activation produced, and show strong  
324 reliability features across two sessions. Each variant also produces a number of useful  
325 readouts (visual, auditory, motor, cognitive/eye-movements) in a wide spatial  
326 distribution across the brain.

327 Both task variants performed similarly for visual, auditory, and motor trials, with robust  
328 activity seen in primary visual, auditory, and motor cortex respectively, and little 'off-  
329 target' activation evident. The eye-movement task also produced a characteristic  
330 pattern of brain activity similar to that seen in previous eye-movement studies (e.g.  
331 Berman *et al*, 1999). The working memory task, though only requiring a very brief (two-  
332 second) retention interval, produced a highly similar pattern of activity to that seen in  
333 more standard working memory tasks such as the N-back task (Owen *et al*, 2005).

334 Importantly, reliability of the tasks was also assessed, and found to be generally high.  
335 Reliability assessment using ICC (or other measures) is still relatively uncommon for  
336 fMRI experiments, but is an important step in validating task paradigms (Caceres *et al*,  
337 2009). The ICC measures obtained here compare very favourably with previous reports  
338 using auditory and working memory tasks (Caceres *et al*, 2009), a cognitive-emotive test  
339 battery (Plichta *et al*, 2012), and a reward task (Fliessbach *et al*, 2010). However, some  
340 task conditions were seen to be more reliable than others. In particular, reliability in the  
341 working-memory variant of the experiment was generally higher than in the eye-  
342 movement variant. One possible explanation for this difference may be due to the  
343 much more cognitively demanding features of the working-memory variant, which led  
344 to a higher level of attention and engagement to all the task conditions in that variant.



345 The high reliability, short duration, and ease of use of these tasks make them ideal for  
346 inclusion as control tasks in pharmacological-MRI studies, as suggested by Iannetti and  
347 Wise (2007), and Bourke and Wall (2015). Inclusion of tasks which are (hypothetically)  
348 unaffected by the drug helps rule out alternative explanations related to systemic drug  
349 effects (on blood pressure, heart-rate, etc.), effects on local vasculature, or neuro-  
350 vascular coupling; all of which can theoretically modulate the BOLD response. One  
351 previous study investigating modulation of amygdala responses by citalopram (Murphy  
352 *et al*, 2009) used a simple checker-board visual control task. Use of a single control task  
353 where activation is restricted to the occipital lobe is sub-optimal as the drug may  
354 potentially still produce non-neural effects in other brain regions. A recent study on the  
355 brain effects of the sex hormone kisspeptin (Comninou *et al*, 2017) used a control task  
356 with a number of readouts in different brain regions (based on Pinel *et al*, 2007). This  
357 task was complex, with ten individual stimulus conditions, different response options,  
358 and contained high-level cognitive stimuli (performing mental arithmetic, reading  
359 sentences on the screen, and listening to recorded voices) which included culture- and  
360 language-specific features. This complexity and the use of language-specific stimuli limit  
361 the broad applicability of this task.

362 The tasks evaluated here represent a good compromise between ease of use, wide  
363 applicability, a short duration, reliable results, and the desirability of providing a number  
364 of readouts in spatially diverse brain regions. While the working memory variant  
365 appears to be somewhat more robust, more reliable, and produces a wider pattern of  
366 brain activity, it is also more cognitively demanding and has significantly more complex  
367 instructions. This may make it less suitable for any patient group with significant  
368 cognitive impairments, who may struggle with a fast, demanding task. The eye-  
369 movement variant may therefore be more suitable for these groups. Additionally, the  
370 eye-movement variant may also be more suitable where the drug under investigation is  
371 hypothesized to have an effect on cognition. In this case, the working-memory variant  
372 may be inappropriate as a control task, as it strongly engages well-known cognitive  
373 brain regions. Either variant would also be suitable for use in a number of other

374 situations where a short, reliable fMRI task that yields a number of readouts is required,  
375 for example in systematic testing of fMRI acquisition sequence parameters (as in  
376 Demetriou *et al*, 2016).

377 We have evaluated two variants of a novel task paradigm, suitable for use as a control  
378 task in pharmacological fMRI studies, or for any use where a general-purpose battery of  
379 basic tasks/stimuli is required. The tasks produce robust brain activation and have  
380 strongly favourable reliability features. The tasks are programmed in an open-source  
381 language and experimental presentation application (Python/Psychopy), and we have  
382 therefore made the stimulus code freely available at  
383 [https://figshare.com/articles/fMRI\\_control\\_task\\_zip/5162065](https://figshare.com/articles/fMRI_control_task_zip/5162065) (DOI:  
384 [10.6084/m9.figshare.5162065](https://doi.org/10.6084/m9.figshare.5162065); Google-generated short-link: [goo.gl/DAqn4V](http://goo.gl/DAqn4V)). We  
385 encourage any interested researchers to download the programs and use them in their  
386 research.

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477 **Acknowledgements**

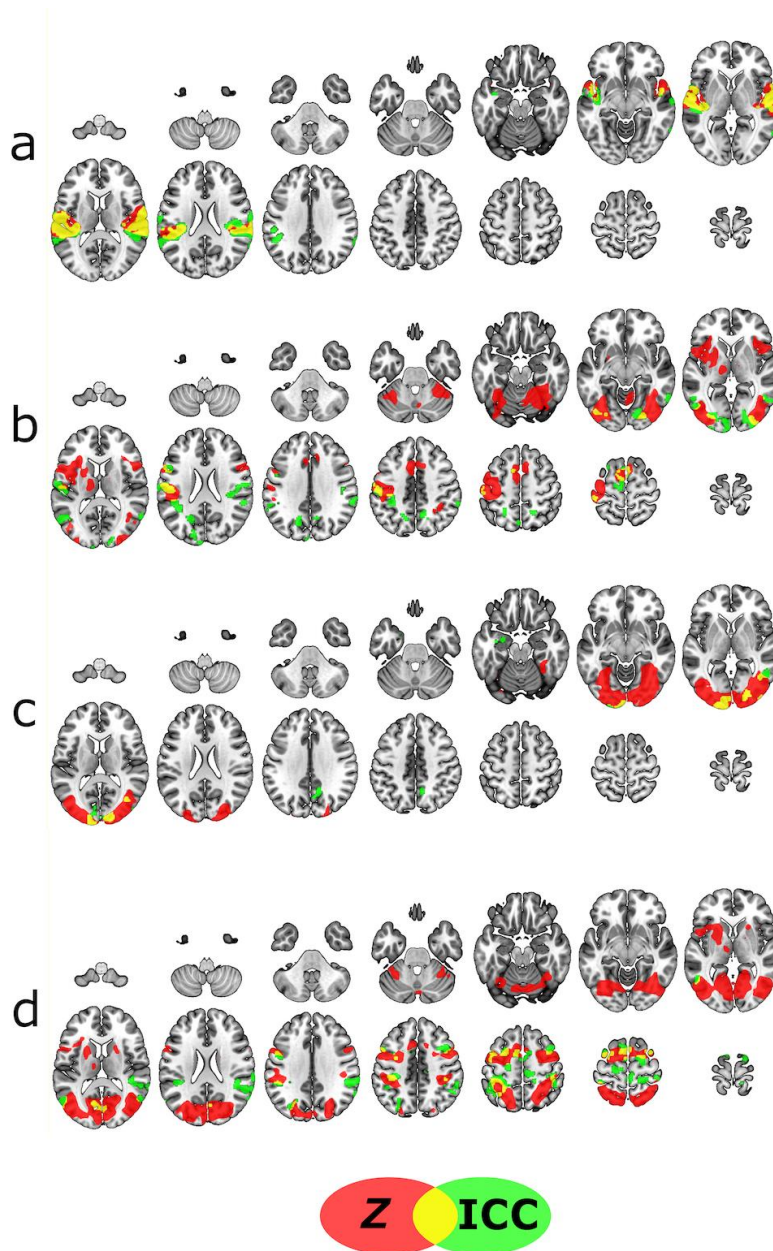
478

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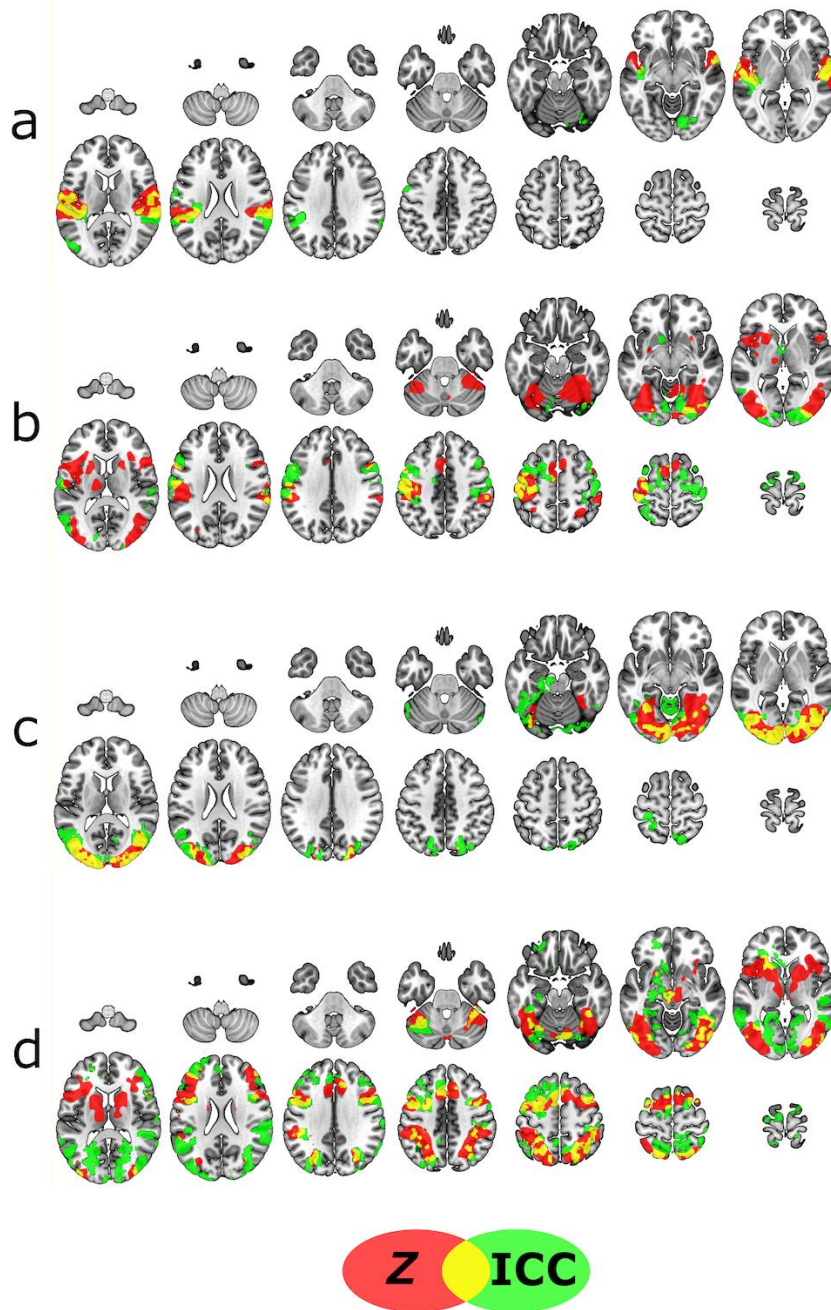
481 general support throughout the investigation

482 **Supplementary information**



483

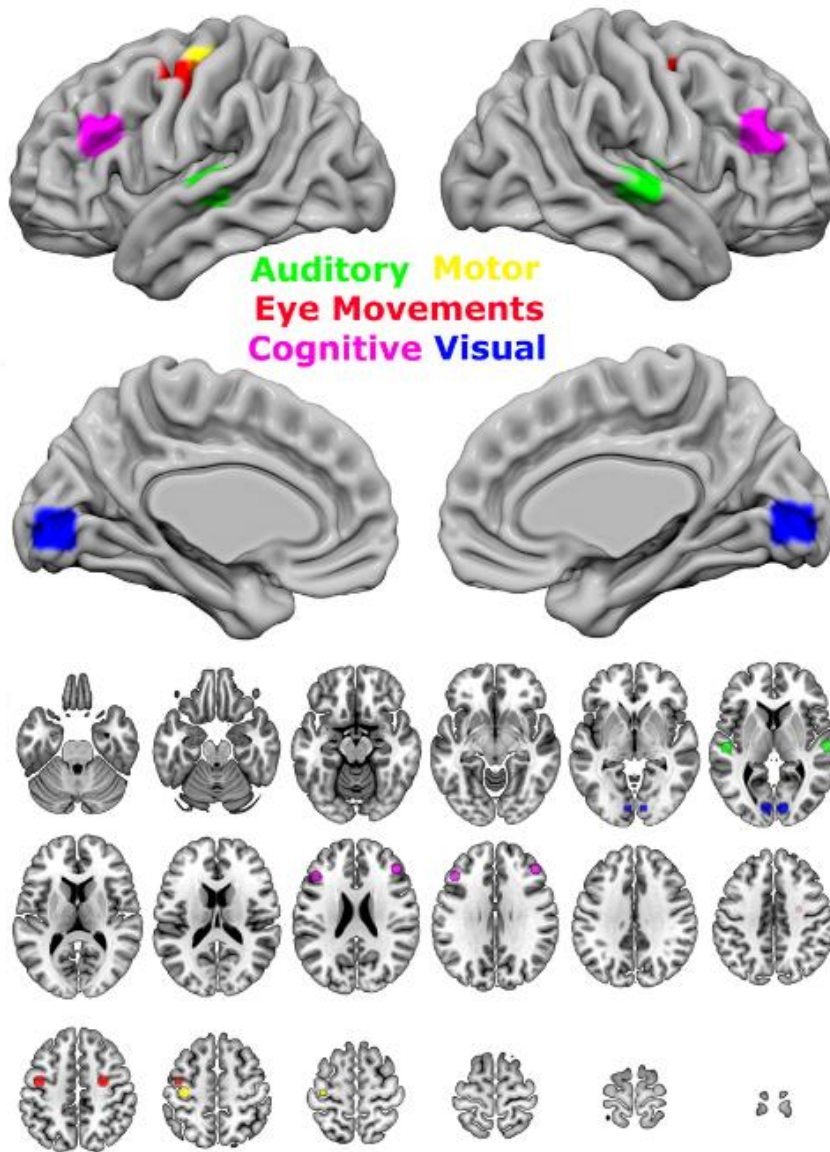
484 Supplementary figure 1. BOLD activation data (Z-scores) and ICC(3,1) reliability values  
485 (both thresholded at  $Z > 3.1$ ,  $p < 0.05$ , cluster-corrected) from the eye-movement  
486 variant represented on the same anatomical image in order to visualize the spatial  
487 relationship between the two sets of data. a) Auditory trials. b) Motor trials. c) Visual  
488 trials. d) Eye movement trials.



489

490 Supplementary figure 2. BOLD activation data (Z-scores) and ICC(3,1) reliability values  
491 (both thresholded at  $Z > 3.1$ ,  $p < 0.05$ , cluster-corrected) from the working-memory  
492 variant represented on the same anatomical image in order to visualize the spatial  
493 relationship between the two sets of data. a) Auditory trials. b) Motor trials. c) Visual  
494 trials. d) Working memory trials.

495



496

497 Supplementary figure 3. Regions used in the ROI analysis visualized on the cortical  
498 surface (upper panel) and on a set of axial slices (lower panel). ROIs were independently  
499 defined as 5mm-radius spheres, using positioning coordinates determined using  
500 guidance from relevant meta-analytic terms on Neurosynth (<http://neurosynth.org/>).