Finding the balance between model complexity and performance: Using ventral striatal

oscillations to classify feeding behavior in rats

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Abstract

The ventral striatum (VS) is a central node within a distributed network that controls appetitive behavior, and neuromodulation of the VS has demonstrated therapeutic potential for appetitive disorders. Local field potential (LFP) oscillations recorded from deep brain stimulation electrodes within the VS are a pragmatic source of neural systems-level information about appetitive behavior that could be used in responsive neuromodulation systems. Here, we recorded LFPs from the bilateral nucleus accumbens core and shell (subregions of the VS) during limited access to palatable food across varying conditions of hunger and food palatability in male rats. We used standard statistical methods (logistic regression) as well as the machine learning algorithm lasso to predict aspects of feeding behavior using VS LFPs. These models were able to predict the amount of food eaten, the increase in consumption following food deprivation, and the type of food eaten. Further, we were able to predict whether the initiation of feeding was imminent up to 42.5 seconds before feeding began and classify current behavior as either feeding or not-feeding. In classifying this behavior, we found an optimal balance between model complexity and performance with models using 3 LFP features primarily from the alpha and high gamma frequencies. As shown here, unbiased methods can identify systems-level neural activity linked to symptoms of mental illness with potential application to the development and personalization of novel treatments.

Author Summary

As neuropsychiatry begins to leverage the power of computational methods to understand disease states and to develop better therapies, it is vital that we acknowledge the trade-offs between model complexity and performance. We show that computational methods can elucidate a neural signature of feeding behavior and show how these methods could be used to discover neural patterns related to other behaviors and used as therapeutic targets. Further, our results helps to contextualize both the limitations and potential of applying computational methods to neuropsychiatry by showing how changing the data being used to

train predictive models (e.g., population vs. individual data) can have a large impact on how

model performance generalizes across time, internal states and individuals.

Introduction

The VS is a central node in the brain circuits influencing goal-directed and habitual

behaviors with subregions like the nucleus accumbens (NAc) core and shell that mediate

information between cognitive control regions of the prefrontal cortex and regions of learning

and memory in the amygdala, hippocampus, and the ventral tegmental area [1-3]. As regions of

convergence within the brain reward circuit, the NAc core and shell have been targeted by

neuromodulation-based treatments for appetitive disorders including substance use disorders,

eating disorders, and obesity [4-6]. Targeting the VS for eating disorders and obesity is

supported by the known connectivity of the NAc with energy homeostasis circuits within the

hypothalamus and brain stem [7,8] and the role of an-/orexigenic states modulating VS activity

through central and peripheral ligands [9-11]. In both preclinical and clinical investigations DBS

targeting these subregions has altered appetitive behavior [12-15], but variable treatment

outcomes combined with the known risks of DBS have limited more widespread use. In other

neuropsychiatric conditions, DBS outcomes have been improved and side-effects limited by

using relevant neural activity to trigger stimulation, closed-loop DBS [16-18], or modify

stimulation parameters, adaptive DBS [19]. However, a source of neural activity that contains

information relevant to appetitive behaviors is needed to apply these advanced DBS

approaches to appetitive disorders.

Local field potential (LFP) oscillations recorded from DBS electrodes are a promising

source of neural systems-level information and VS oscillations could contain information about

appetitive behavior. Although there has been evidence that high frequency components of NAc

LFPs could be generated within the piriform cortex [20] the entrainment of single-unit firing to

LFPs in the NAc suggests that VS LFPs are, at a minimum, a reflection of local striatal

processing [21-23]. Therefore, it is likely that LFPs recorded from the NAc contain information

pertaining to reward related behaviors.

Although a wealth of information likely exists within VS LFPs about appetitive behaviors

like binge eating, it is important to determine how much information is needed to decode these

behaviors and to determine what the trade-offs are between model performance and model

simplicity. The model used by Wu et al. [18] took advantage of changes in delta power during

the beginning of feeding in mice to trigger closed-loop DBS and reduced binge size. This is a

good example of a low complexity population-based model (1 LFP feature trained from 6

animals) maximizing simplicity at the expense of performance (69% sensitivity and 64%

specificity). Our work examined how altering model complexity changes performance in

classifying feeding behavior in a rat model of binge eating. Unbiased statistical and machine

learning approaches were used to predict imminent binge eating epochs and classify concurrent

behavior using LFP recordings from bilateral NAc core and shell. Further, we used a machine

learning approach to determine if VS oscillations recorded during binge eating sessions

contained information that could predict the quantity of food consumed, the increase in binge

size following food deprivation, or the type of food consumed (low vs. high palatability).

Primarily, this work characterizes how different sets of training data (complex vs. simple;

individualized vs. population-based) can affect the performance of models across individuals,

time, and internal conditions. Although shown here in a rat model of binge eating, we expect

these relationships to generalize to other appetitive behaviors and neuropsychiatric disorders,

thus providing a framework for the development of more effective closed-loop algorithms and

adaptive neuromodulation-based treatments.

Materials and Methods

Male Sprague-Dawley rats (n = 12) were purchased from Charles River (Shrewsbury,

MA) at 60 days of age were individually housed using a reverse 12-hour light/dark schedule with

house chow and water available *ad libitum*. All experiments were carried out in accordance with

the NIH Guide for the Care and Use of Laboratory Animals (NIH Publications no. 80-23) revised

in 1996 and approved by the Institutional Animal Care and Use Committee at Dartmouth

College.

Experimental design

All animals were implanted with electrode arrays and were conditioned to binge eat

using limited access to palatable food (1 month). Following completion of a DBS intervention

published separately [24] and a 2 week washout period, rats re-established a baseline of binge-

like feeding. Once a stable baseline was established, baseline binge sessions (Base) were

recorded (LFP and video). Binge sessions were also recorded following 24- and 48-hour food

deprivation (Dep 24 and Dep48) with intervening periods (at least 24 hours) of *ad libitum* access

to house chow. Animals were also deprived of food for 24 hours before recording a 2-hour

house chow session (Chow) to ensure that the animals consumed enough food to provide a

comparable amount of LFP data during feeding to the three sessions with access to the high-

fat/high-sugar diet (See General Methods: Surgery and Binge Eating).

These paired LFP and video recordings were used to address two types of questions: 1)

Whole session questions—can VS activity averaged over an entire session be used to predict

behavioral outcomes from that session (e.g., predict calories consumed)?; and 2) **Within**

session questions—can VS activity be used to classify behavior as it occurs or to predict if it is

about to occur? These two types of questions were assessed using tailored analysis

approaches that have different sample size considerations and will be described in the

corresponding subsections of Statistical Analysis.

General methods

Surgery and binge eating

Following habituation to the animal facility, rats were anesthetized with

isoflourane/oxygen (5% isoflourane for induction and 2% for maintenance) and underwent

stereotaxic implantation with a custom electrode array targeting both the NAc core and shell

bilaterally: 1.6 mm anterior; ±1 and 2.5 mm lateral; and 7.6 mm ventral to bregma. Following

recovery from surgery (~1 week), rats began a well described [25-27] schedule of limited access

to a palatable high-fat/high-sugar diet (sweet-fat food), which contained 4.6 kcal/g and 19%

protein, 36.2% carbohydrates, and 44.8% fat by calories (Teklad Diets 06415, South Easton,

MA). The sweet-fat food was provided to the rats in addition to house chow and water within

stimulation chambers for 2-hour sessions with 4-5 sessions irregularly spaced per week.

Behavioral measures

The food was weighed before and after all recording sessions to calculate the amount of

food consumed during the session; weight was converted to kilocalories to allow direct

comparison between food types (sweet-fat food vs. house chow). Session videos were manually

scored for feeding, approach (movement towards food), and rest intervals. Timestamps were

normalized by session length in order to compare feeding dynamics across sessions of unequal

length (see Supplemental Methods: Behavioral measures).

Local field potential recording and processing

Rats were tethered in an 18"x12"x24" chamber through a commutator to a Plexon data

acquisition system while time-synchronized video was recorded (Plexon, Plano, TX) for offline

analysis. All LFP signal processing was done using custom code written from Matlab R2017a as

previously reported [24] (see Supplemental Methods: Signal processing).

Verification of electrode placement

Rats were euthanized at the end of the experiment using CO_2. Brains were removed,

sectioned with a cryostat, mounted on slides, and stained with thionine for histologic verification

of electrode placement [15]. No animals required exclusion based on electrode location.

Statistical analysis - Whole session

To determine how much of the individual heterogeneity in feeding behavior could be

predicted from VS activity, the values of each LFP feature were averaged across all bins

according to behavioral scoring (i.e., feeding vs. resting) from a given session. To compare

across animals and to account for day-to-day variation in signal fluctuations the LFP features

were normalized by subtracting the average feeding value from the average rest value (Figure

2A). These rest-normalized LFP features were then used to predict behavioral variables

(baseline food intake and food type). To predict the change in consumption with food

deprivation—from Base to Dep24 or Dep48 session—the difference between the rest-

normalized values of the two sessions were used as predictor variables (e.g., Base[feeding-rest]

- Dep24[feeding-rest]). Although there were only 12 animals, by using up to two recordings per

animal sample sizes were able to be increased ($n = 24$ for both baseline food intake and change

in consumption with food deprivation; $n = 21$ for food type, one animal didn't have any house

chow sessions and another only had one); however, lasso is specifically for regressions in

which p >> n and thus these samples size only limited the number of folds used in cross-

validation.

The Matlab package *Glmnet* [28] was used to implement lasso with 100 iterations of 5-

fold cross-validation. Since there were insufficient samples to construct a naïve test-set, model

performance was estimated from the distributions of performances during cross-validation. For

predicting baseline food intake and the change in consumption from baseline (continuous

outcomes) performance was estimated as mean absolute error (MAE) and for predicting food

type (binary outcome) performance was estimated as accuracy (%), both performance

measures were reported with 95% confidence intervals. The performance distributions from

cross-validation were then compared to distributions representing by-chance performance

created by shuffling the assignment of predictor and outcome variables using Monte Carlo

sampling. The actual and permuted distributions were compared using the Mann-Whitney *U* test

and the *U* test statistic was converted into a Cohen's *d* (Supplemental Methods: Effect size).

Statistical analysis - Within session

Each 5-second bin and its corresponding LFP features belonged to only one behavioral

category: feeding, pre-feeding, or not-feeding. Pre- and not-feeding were not manually scored;

rather bins were assigned to those categories relative to the scored timestamps. Pre-feeding

bins were defined as those occurring 45 seconds prior to feeding initiation and were discarded if

they overlapped with a previous feeding epoch. All bins that were neither feeding nor pre-

feeding were categorized as 'not-feeding'.

Training pre-feeding vs. not-feeding models

Pre-feeding vs. not-feeding models were first trained and tested using pre-feeding bins

that immediately preceded the start of feeding to determine if brain activity immediately before

feeding was differentiable from brain activity during other behaviors. These models were then

also tested on pre-feeding bins centered up to 45 seconds before feeding (Figure 3A). To

account for the variability introduced through random sub-sampling and imputation of the bins

used, all of these steps were repeated 20 times and the performance reported as averages with

95% confidence intervals (see Supplemental Methods: Pre-feeding vs. not-feeding).

Training feeding vs. not-feeding models

Logistic regressions, fit using the Matlab function *fitglm()*, were used to train models to

classify bins as feeding or not-feeding (see Supplemental Methods: Feeding vs. not-feeding).

The process of imputing and splitting the data into test and training sets was repeated 20 times

for each condition (Base, Dep24, Dep48, and Chow).

Evaluating model performances

Model performances were measured using the naïve test-sets to calculate the

classification probabilities of the new data with the function *predict()*, constructing a receiver

operator characteristic (ROC) curve and calculating the area under the ROC curve (AUC) with

the function *perfcurve()*. Performance was then averaged over the 20 iterations and reported

with 95% confidence intervals. As before, Monte Carlo sampling used to shuffle the assignment

of predictor and outcome variables in order to assess by-chance accuracy and the effect size

between the distributions of actual and permuted performances was calculated by converting

the *U* test statistic into a Cohen's *d* (see Supplemental Methods: Effect size).

Relating model complexity to performance

The complexity of models used to differentiate brain activity during feeding from brain

activity during not-feeding was adjusted across three domains: 1. the number of individual

animals included; 2. the number of LFP features included; and 3. the number of conditions

represented (Base, Dep24, Dep48, and Chow). Two-sample t-tests were used to compare the

performance between models with different manipulations of the following domains followed by

the Bonferroni correction.

1. Individuals: To determine how many individual animals were required to create a

population-based model that could generalize across animals, all permutations from 1/12 to

11/12 animals were used to train models. Population models (>1 animal used to train the model)

were tested on the data of left-out animal(s) (see Supplemental Methods: Complexity vs.

performance).

2. LFP Features: The performance of the logistic model built from all LFP features was

considered the "gold standard" for determining how many features were required to create a

model that was stable across individuals and conditions. The lasso algorithm reduced the

number of features used to ~40. To test the lower bounds of simplicity, the performance of

logistic models built from all possible permutations of up to three features: 58 monads, 1,653

dyads, and 30,856 triads. "Top-tier" models were those with performances not significantly

different from the best performing model within each group as assessed using two-sample t-

tests followed by the Bonferroni correction for multiple comparisons (i.e., top-tier monad models

were monad models that did not perform significantly worse than the best monad model).

3. Conditions: Models were trained using data from either just baseline or all four

conditions, but in both cases more bins were used than needed to achieve stable model

performance as determined by learning curves (Figure S2; see Supplemental Methods:

Complexity vs. performance).

Visualizing LFP feature changes around feeding epochs

Features of interest (from monad, dyad, and triad models) were extracted from all

recordings around feeding epochs from 62.5 seconds before feeding to 32.5 seconds into

feeding, and from 12.5 seconds before feeding ended to 52.5 seconds after feeding ended

(feeding epochs were only used if they lasted at least 45 seconds to avoid using data twice). For

times outside of feeding, only data that did not overlap with previous or subsequent feeding

epochs were used. The data from all baseline recordings were used to calculate the average

LFP feature value in each 5 second bin around feeding epochs and were plotted through time

with one standard deviation.

Results

<u>Whole session results</u>

Characterization of feeding dynamics across session types

There was a bimodal pattern of feeding behavior during the baseline conditions that was

not maintained across the food deprived conditions (Figure 1A) in which more animals were

feeding during the beginning of the recording. The temporal dynamics of feeding in animals

given house chow after 24 hours of food deprivation was more similar to the deprived animals

given palatable food rather than baseline; however, during the Chow condition the animals ate

significantly fewer calories than both Dep24 and Dep48 conditions (t(19) = 3.73, p = .008, two-

sample t-test; and t(16) = 5.82, p = .0002, two-sample t-test; Figure 1B). During the sweet-fat

food sessions, 48 hours of food deprivation were required to significantly increase the number of

calories consumed compared to baseline (t(19) = -4.25, p = .003, two-sample t-test; Figure 1B).

Decoding the amount of food consumed and food type from VS oscillations

Using the brain activity at rest recorded during baseline sessions (Figure 1C) models

were built that outperformed permuted data in predicting the amount of food eaten at baseline

(MAE = 2.6±0.08 gm; d = 0.43; Figure 1D). Next, changes in brain activity at rest from Base to

Dep24 or to Dep48 were used to predict the changes in the amount of food consumed across

the corresponding sessions (MAE = 0.8±0.01%; d = 1.1; Figure 1E). Last, brain activity at rest

was used to predict the type of food being eaten following 24-hour food deprivation—house

chow vs. sweet-fat food (accuracy = 59±1%; d = 0.55; Figure 1F).

<u>Within session results</u>

Predicting imminent feeding

LFP features from the bins immediately preceding feeding epochs in the baseline

session were used to build models (Figure 2A) that predicted whether initiation of feeding was

imminent (AUC = 0.81±0.03; d = 2.68; Figure 2B). When these models were applied backwards

through time, they were able to successfully differentiate bins as preceding feeding (i.e. pre-

feeding bins centered up to 42.5 seconds before feeding began) from all other bins outside of

feeding epochs (Figure 2C). These models were not merely detecting approach behavior since

only one third of the pre-feeding bins had any overlap with approach behavior and none of the

bins more than 12.5 seconds before feeding overlapped with approach while the model was still

able to differentiate beyond 12.5 seconds (Figure 2D).

The identity of the LFP features that were most frequently used by lasso to predict

imminent feeding were plotted over time to investigate the temporal link between changes in

these LFP features and feeding behavior. Both a power (shell left high gamma; Figure 2E) and

coherence feature (core left-core right high gamma; Figure 2F) tended to transition from the

non-feeding average towards the feeding average during the pre-feeding interval (42.5 seconds

before feeding). After feeding ceded, the LFP features began to transition back to their non-

feeding level.

<u>Relating model complexity to performance using models classifying feeding vs. not-feeding</u>

To explore model complexity, three domains of the data used for model building were

manipulated (Figure 3A): number of individuals, number of LFP features, and number of

conditions (Base, Dep24, Dep48, and Chow). By using the same naïve test-sets for assessing

performance, the effects of different training data could be directly on performance could be

compared directly.

Manipulation of the number of animals in population-based models

Population-based models built from and tested on data from all animals was able

distinguish brain activity during feeding from not-feeding better than would be expected by

chance alone (AUC = 0.87±0.01; d = 3.27; Figure 3Bi). All models were built using 80% of each

individual animal's data from baseline sessions (Figure 2A) and the models were tested on the

left-out 20%. However, it is conceivable that because the left-out 20% came from the same

recordings as the 80% used for training, these models could be slightly overfit. To account for

this a leave-one-out (LOO) approach was used by leaving an entire animal out of the model

building to be used as the test-set. As expected, the performance of LOO models decreased

significantly (t(258) = 2.96 p = .003, two-sample t-test), but they still outperformed the by-chance

permuted models (AUC = 0.78±0.06; d = 3.13; Figure 3Bi). As the number of animals left out

was increased (Figure 3Bi Inset) the performance continued to decline (Figure 3C).

Individualized vs. population-based models

The above data indicate that if enough individuals are used to train population-based

models, then the model will generalize across individuals, outperforming chance. It is possible

however that a model built from an individual will be able to perform better for that individual

compared to a model built from a population. To test this individualized models were built using

80% of a single animal's data and then tested on that animal's left-out 20%. These models

performed better than the permuted models (AUC = 0.89±0.06; d = 3.13; Figure 3Bii) and

performed better than the population-based models tested on the same left-out data in 9/12

individuals when all animals were in a population model (Figure 3 Biii All) and 11/12 individuals

when all but that individual was used to train the population-based model (Figure 3Biii LOO).

Manipulation of the number of LFP features at baseline

The next step was to determine how many LFP features are necessary to build

successful and stable models by manipulating the number of features included in model building

from all single feature models to all three feature models (Figure 4A Inset). When classifying

baseline feeding vs. not-feeding, the best models built from a single feature performed better

than chance and although increasing the number of features used to two or three increased

performance, these simple models never achieved the performance of either the lasso (~40

features) or full logistic (58 features) model (Figure 4A). Further, when these simpler models

were applied to testing data from the other conditions (Dep24, Dep48, and Chow) the

performance dropped with the more complex triadic models providing the best performance

stability across conditions, approaching the stability of the full logistic models (Figure 4B). Last,

the features used by the best dyad and triad models and those used by lasso were not all top

performing features when used in monadic models, suggesting redundancy between LFP

features in predicting feeding behavior (Figure S4).

Manipulation of conditions used to train and test models: impact on individual and population

model performance

Given that individualized models tended to outperform population-based models when

trained and tested in the baseline condition the performance of these models was also

determined when data from the other three conditions were used as the test-set. The

population-based models significantly outperformed the individual models (Dep24 $t(26)$ = -4.03,

p = .0035; Dep48 $t(26)$ = -3.53, p = .012; and Chow $t(26)$ = -3.63, p = .0097; Figure 5A). To

determine if the model performances could be improved across the conditions, new

individualized and population-based models were built using data from all four conditions

(Figure 5A Inset). These individualized models significantly outperformed the population-based

models (Base $t(26)$ = 3.56, p = .012; Dep24 $t(26)$ = 3.94, p = .0044; and Dep48 $t(26)$ = 9.69, p =

3.3E-9; Chow $t(26)$ = 3.52, p = .013; Figure 5B). In summary, the population-based models built

from the baseline condition generalized better across the other conditions compared to the

individualized models. However, if individualized models are trained on data from all conditions,

then they can outperform the population-based models in classifying feeding vs. not-feeding

across conditions.

 Manipulation of the number of LFP features used to build models across conditions

Finally, the above findings were integrated by determining the minimal number of LFP

features required in an individualized model built from all conditions to match the performance of

the corresponding, "gold standard", logistic model using all 58 LFP features (Figure 6 Inset).

Testing on Base and Chow data revealed that only two features were required to attain a

performance that was not significantly different from the gold standard logistic model (Base t(14)

= 3.07, p = .13; Chow t(14) = 1.74, p = 1; Figure 6A and D). The Dep24 condition required 48

features used by lasso (Dep24 t(14) = 3.19, p = .10; Figure 6B) to perform at a comparable level

to the full logistic. However, testing all possible combinations of LFP features from 4 to 48 was

beyond the computational capacity of this study.

When data from all conditions were used from training and testing it was found that

many of the models performed equally well (Table S1). Despite the flexibility in the exact

features used in these models, features within the alpha and high gamma ranges were the most

common contributors to the top performing models (Table 1). For the simpler models—monads

and dyads—most predictors were power features while in the more complex triads coherence

features became equally represented (Table S1).

Table 1: Frequency contributions in top performing monad, dyad, and triad models.

	Monad	Dyad	Triad
Delta	—	38%	44%
Theta	—	—	—
Alpha	50%	88%	84%
Beta	—	13%	13%
Low Gamma	—	—	44%
High Gamma	50%	63%	72%

Discussion

Here we show that VS oscillations can be decoded and used to predict aspects of

feeding behavior such as the amount and type of food consumed. Further, these oscillations

can be used in real-time to predict imminent or current feeding in a rat model of binge eating,

regardless of varying hunger levels and food palatability. By manipulating the complexity of the

training data used and then assessing how these manipulations affect model performance, this

work creates a theoretical framework to guide the implementation of predictive algorithms used

in closed-loop and adaptive neuromodulation systems. Specifically, this work suggests that

devices could be pre-loaded with a model built from a group of individuals using a handful of

oscillatory features and have fair performance when applied to individuals outside of the training

group. However, to achieve optimal performance in a specific individual, personalized models

using neural data from that individual acquired over time would be needed.

<u>Predicting amount of food consumed and food type from VS oscillations</u>

The binge eating model used in this study resulted in variation in food intake between

individuals (as previously described, [29]) and also in the increased intake following food

deprivation. That this variation could be partially predicted using LFP features from the VS is not

surprising given the connectivity of these VS regions (e.g., nucleus accumbens) to the

distributed feeding network [30,31]. Further, it is feasible that information about the type of food

consumed (low vs. high palatability) could also be extracted from VS oscillations given that

'liking' of food [32,33] and nutritive/caloric value [34] are processed by the NAc.

<u>Population-based vs. individualized models</u>

The presented data suggest that models classifying feeding behavior perform best when

they are built and tested within a given individual and condition, otherwise performance drops

when these individualized models are tested in other conditions—even if within the same

animal. However, this drop can be mitigated in two ways: 1. use data from multiple conditions

within an individual; or 2. use data from multiple individuals within a condition (or from multiple

conditions). Following either of these strategies will increase the probability of selecting and

properly weighting LFP features that generalize across animals and conditions. Clinically, it is

important that models are able to perform well across a heterogeneous population as well as

across the variable conditions through which individuals will transition over time. Therefore,

when building models for use in algorithms that control closed-loop or adaptive neuromodulation

systems it will be vital to consider these strategies.

Machine learning and DBS

Recently, there has been increasing interest in applying machine learning and other

computational methods to guide the selection and implementation of psychiatric treatments.

This work can be categorized into three domains: 1. predicting treatment outcomes, 2. defining

treatment parameters, and 3. actively optimizing treatment through time. Treatment outcomes

have been successfully predicted using both structural and functional connectivity measures in

Parkinsonian patients [35] as well as using LFPs in a rodent model of binge eating [24]. In a

high throughput manner, machine learning has also been used to optimize combinations of DBS

parameters and medications [36] and to determine which DBS parameters lead to desired

changes in brain activity [37]. Last, there is a push towards the development of neuromodulation

systems that use machine learning to monitor stimulation evoked dopamine signaling and

adjusting stimulation parameters to optimize treatment [38] or to determine the time and brain

state during which stimulation has the largest effect [39]. With the exception of Kumar et al.'s

work, all of these implementations of machine learning used population-based datasets (i.e.

data pooled across subjects). For some predictions—e.g., optimizing stimulation target—using

individual datasets is impractical; however, when tuning stimulation parameters or trying to

determine effective stimulation timing our work suggests individualized data will produce the

best models, if those data were sampled from across time and, ideally, across varying

conditions (e.g., stress/anxiety, mood, hunger, etc.).

Number of predictors required for stable performance

This work highlights an important trade-off between the number of features used to build

a model and that model's performance across individuals and conditions. Our results suggest

that single feature models are unlikely to perform with enough accuracy to be clinically useful.

However, a relatively simple model (~3 features) can approach the performance and stability of

complex models (58 features); although these exact numbers may vary when predicting

different behaviors/symptoms, this work suggests that simpler models can contain enough

information pertaining to a given behavior/symptom with the benefit of limiting the computational

and power requirements.

A predictable pattern of brain activity precedes feeding initiation

As shown (Figure 2), VS oscillations can differentiate times when an animal is about to

feed (≤45 seconds before feeding begins) from not-feeding. Interestingly, models built to classify

feeding were also able to classify pre-feeding—even slightly outperforming pre-feeding models.

This was because although many of the same LFP features were used in both models, the

features are more clearly delineated (i.e., higher signal to noise ratio) between feeding and not-

feeding, likely representing a "ramping" of LFP features as feeding begins.

When this hypothesis was examined (Figure 2E and F), a ramping phenomenon was

observed in features that more successfully classified pre-feeding bins when trained on feeding

vs. not-feeding data. For example, NAc shell left high gamma power begins to increase to its

feeding level before feeding begins, stabilizes during feeding, then drops back to not-feeding

levels as feeding ends. In other features there is decreased variance during feeding (Figure 2-

2), mirroring a widespread cortical pattern seen in response to obtaining rewards [40], as a

marker of stimulus perception/detection [41,42], and has been correlated with performance on

visual discrimination [43,44] and motor preparation/initiation [45,46]. Visualizing several of these

LFP features over time makes it clear that they develop over different timescales, likely

underpinning the accuracy of predicting imminent feeding increasing closer to the start of

feeding as more features have diverged from their not-feeding levels (Figure 2C).

Confounds and noise

Given that motor preparation and initiation manifest as decreased neural variability it is

possible that the models predicting imminent feeding were merely detecting the motor activity of

approaching the food. However, by 12.5 seconds before feeding none of the data used for

model building contained approach behavior (Figure 2D) and the models were able to classify

pre-feeding brain activity out to 42 seconds before feeding without a corresponding drop in

performance at 12.5 seconds (Figure 2C). When models were built using feeding data—with no

approach behavior—performance was actually slightly better at classifying pre-feeding.

Together these results suggest that although approach behavior may also exhibit a detectable

change in LFPs, this change is not a primary source of information for our models.

There is also a concern that without electromyography of the masseters we are unable

to completely remove the possibility of chewing noise influencing models built from feeding data.

However, if the feeding vs. not-feeding models were chewing detectors, then the models should

only be able to detect behaviors with chewing noise. Instead the feeding models were also able

to classify pre-feeding activity which is devoid of chewing noise.

VS oscillations as a source of information for closed-loop and adaptive neuromodulation

Appetitive disorders like binge eating disorder have been associated with dysregulation

of the brain reward circuit which includes the VS. Understanding the nature of network

pathology is critical to the development of treatments that can therapeutically alter network

activity, ameliorating the problematic behavior/symptom. Neuromodulation-based interventions

that use network activity to trigger stimulation and modify parameters have proven effective in

the treatment of Parkinson's disease [19]. DBS for epilepsy has incorporated electrodes in order

to detect pre-seizure electrophysiologic activity and use stimulation to prevent seizure

generation [16]. Future treatments of appetitive disorders could similarly utilize meaningful

electrophysiology features in order to provide feedback to optimize treatment efficacy and limit

the side effect profile. A recent study demonstrated the theoretical feasibility of using a closed-

loop system to trigger stimulation and decrease binge size in a mouse model of binge eating

[18]. As noted in the introduction, the model used had limited performance, likely due to only

using a single LFP feature, but the success of the intervention highlights another point to

consider when determining model complexity vs. model performance tradeoffs: what model

performance is required to meaningfully impact the outcome of interest?

Conclusions

Ventral striatal oscillations can predict feeding behavior during sessions of limited

access to palatable food in rats. Similar unbiased computational methods will continue to

identify new systems-level neural markers and produce models capable of predicting behaviors

that are relevant to an array of neuropsychiatric conditions.

References

1. Berridge KC, Ho CY, Richard JM, DiFeliceantonio AG (2010) The tempted brain eats:

pleasure and desire circuits in obesity and eating disorders. Brain Res 1350: 43-64.

2. Ferrario CR, Labouebe G, Liu S, Nieh EH, Routh VH, et al. (2016) Homeostasis Meets

Motivation in the Battle to Control Food Intake. J Neurosci 36: 11469-11481.

3. Volkow ND, Wang GJ, Fowler JS, Tomasi D, Baler R (2012) Food and drug reward:

overlapping circuits in human obesity and addiction. Curr Top Behav Neurosci 11: 1-24.

4. Muller UJ, Voges J, Steiner J, Galazky I, Heinze HJ, et al. (2013) Deep brain stimulation of

the nucleus accumbens for the treatment of addiction. Ann N Y Acad Sci 1282: 119-128.

5. Pierce RC, Vassoler FM (2013) Deep brain stimulation for the treatment of addiction: basic

and clinical studies and potential mechanisms of action. Psychopharmacology (Berl)

229: 487-491.

6. Kumar R, Simpson CV, Froelich CA, Baughman BC, Gienapp AJ, et al. (2015) Obesity and

deep brain stimulation: an overview. Ann Neurosci 22: 181-188.

7. Carus-Cadavieco M, Gorbati M, Ye L, Bender F, van der Veldt S, et al. (2017) Gamma
oscillations organize top-down signalling to hypothalamus and enable food seeking.
Nature 542: 232-236.
8. Leigh SJ, Morris MJ (2016) The role of reward circuitry and food addiction in the obesity
epidemic: An update. Biol Psychol.
9. Berendse HW, Groenewegen HJ, Lohman AH (1992) Compartmental distribution of ventral
striatal neurons projecting to the mesencephalon in the rat. J Neurosci 12: 2079-2103.
10. Zahm DS, Brog JS (1992) On the significance of subterritories in the "accumbens" part of
the rat ventral striatum. Neuroscience 50: 751-767.
11. Groenewegen HJ, Wright CI, Beijer AV (1996) The nucleus accumbens: gateway for limbic
structures to reach the motor system? Prog Brain Res 107: 485-511.
12. Vassoler FM, Schmidt HD, Gerard ME, Famous KR, Ciraulo DA, et al. (2008) Deep brain
stimulation of the nucleus accumbens shell attenuates cocaine priming-induced
reinstatement of drug seeking in rats. J Neurosci 28: 8735-8739.
13. Liu Y, Postupna N, Falkenberg J, Anderson ME (2008) High frequency deep brain
stimulation: what are the therapeutic mechanisms? Neurosci Biobehav Rev 32: 343-351.
14. Knapp CM, Tozier L, Pak A, Ciraulo DA, Kornetsky C (2009) Deep brain stimulation of the
nucleus accumbens reduces ethanol consumption in rats. Pharmacol Biochem Behav
92: 474-479.
15. Doucette WT, Khokhar JY, Green AI (2015) Nucleus accumbens deep brain stimulation in a
rat model of binge eating. Transl Psychiatry 5: e695.
16. Morrell MJ, Group RNSSiES (2011) Responsive cortical stimulation for the treatment of
medically intractable partial epilepsy. Neurology 77: 1295-1304.
17. Rosin B, Slovik M, Mitelman R, Rivlin-Etzion M, Haber SN, et al. (2011) Closed-loop deep
brain stimulation is superior in ameliorating parkinsonism. Neuron 72: 370-384.

18. Wu H, Miller KJ, Blumenfeld Z, Williams NR, Ravikumar VK, et al. (2017) Closing the loop

on impulsivity via nucleus accumbens delta-band activity in mice and man. Proc Natl

Acad Sci U S A.

19. Little S, Pogosyan A, Neal S, Zavala B, Zrinzo L, et al. (2013) Adaptive deep brain

stimulation in advanced Parkinson disease. Ann Neurol 74: 449-457.

20. Carmichael JE, Gmaz JM, van der Meer MAA (2017) Gamma Oscillations in the Rat Ventral

Striatum Originate in the Piriform Cortex. J Neurosci 37: 7962-7974.

21. van der Meer MA, Redish AD (2009) Low and High Gamma Oscillations in Rat Ventral

Striatum have Distinct Relationships to Behavior, Reward, and Spiking Activity on a

Learned Spatial Decision Task. Front Integr Neurosci 3: 9.

22. Tort AB, Komorowski RW, Manns JR, Kopell NJ, Eichenbaum H (2009) Theta-gamma

coupling increases during the learning of item-context associations. Proc Natl Acad Sci

U S A 106: 20942-20947.

23. Howe MW, Atallah HE, McCool A, Gibson DJ, Graybiel AM (2011) Habit learning is

associated with major shifts in frequencies of oscillatory activity and synchronized spike

firing in striatum. Proc Natl Acad Sci U S A 108: 16801-16806.

24. Doucette WT, Dwiel L, Boyce JE, Simon AS, Khokhar JY, et al. (2018) Machine learning

based classification of deep brain stimulation outcomes in a rat model of binge eating

using ventral striatal oscillations Front Psychiatry.

25. Berner LA, Avena NM, Hoebel BG (2008) Bingeing, self-restriction, and increased body

weight in rats with limited access to a sweet-fat diet. Obesity (Silver Spring) 16: 1998-

2002.

26. Corwin RL (2004) Binge-type eating induced by limited access in rats does not require

energy restriction on the previous day. Appetite 42: 139-142.

27. Corwin RL, Buda-Levin A (2004) Behavioral models of binge-type eating. Physiol Behav 82:

123-130.

28. Friedman J, Hastie T, Tibshirani R (2010) Regularization Paths for Generalized Linear

535   Models via Coordinate Descent. J Stat Softw 33: 1-22.

536   29. Boggiano MM, Artiga AI, Pritchett CE, Chandler-Laney PC, Smith ML, et al. (2007) High

537   intake of palatable food predicts binge-eating independent of susceptibility to obesity: an

538   animal model of lean vs obese binge-eating and obesity with and without binge-eating.

539   Int J Obes (Lond) 31: 1357-1367.

540   30. Castro DC, Cole SL, Berridge KC (2015) Lateral hypothalamus, nucleus accumbens, and

541   ventral pallidum roles in eating and hunger: interactions between homeostatic and

542   reward circuitry. Front Syst Neurosci 9: 90.

543   31. Urstadt KR, Stanley BG (2015) Direct hypothalamic and indirect trans-pallidal, trans-

544   thalamic, or trans-septal control of accumbens signaling and their roles in food intake.

545   Front Syst Neurosci 9: 8.

546   32. Shin AC, Pistell PJ, Phifer CB, Berthoud HR (2010) Reversible suppression of food reward

547   behavior by chronic mu-opioid receptor antagonism in the nucleus accumbens.

548   Neuroscience 170: 580-588.

549   33. Pecina S, Berridge KC (2000) Opioid site in nucleus accumbens shell mediates eating and

550   hedonic 'liking' for food: map based on microinjection Fos plumes. Brain Res 863: 71-86.

551   34. de Araujo IE, Oliveira-Maia AJ, Sotnikova TD, Gainetdinov RR, Caron MG, et al. (2008)

552   Food reward in the absence of taste receptor signaling. Neuron 57: 930-941.

553   35. Horn A, Reich M, Vorwerk J, Li N, Wenzel G, et al. (2017) Connectivity Predicts deep brain

554   stimulation outcome in Parkinson disease. Ann Neurol 82: 67-78.

555   36. Shamir RR, Dolber T, Noecker AM, Walter BL, McIntyre CC (2015) Machine Learning

556   Approach to Optimizing Combined Stimulation and Medication Therapies for Parkinson's

557   Disease. Brain Stimul 8: 1025-1032.

37. Heldman DA, Pulliam CL, Urrea Mendoza E, Gartner M, Giuffrida JP, et al. (2016)

Computer-Guided Deep Brain Stimulation Programming for Parkinson's Disease.

Neuromodulation 19: 127-132.

38. Grahn PJ, Mallory GW, Khurram OU, Berry BM, Hachmann JT, et al. (2014) A

neurochemical closed-loop controller for deep brain stimulation: toward individualized

smart neuromodulation therapies. Front Neurosci 8: 169.

39. Kumar SS, Wulfing J, Okujeni S, Boedecker J, Riedmiller M, et al. (2016) Autonomous

Optimization of Targeted Stimulation of Neuronal Networks. PLoS Comput Biol 12:

e1005054.

40. Churchland MM, Yu BM, Cunningham JP, Sugrue LP, Cohen MR, et al. (2010) Stimulus

onset quenches neural variability: a widespread cortical phenomenon. Nat Neurosci 13:

369-378.

41. Schurger A, Pereira F, Treisman A, Cohen JD (2010) Reproducibility distinguishes

conscious from nonconscious neural representations. Science 327: 97-99.

42. Schurger A, Sarigiannidis I, Naccache L, Sitt JD, Dehaene S (2015) Cortical activity is more

stable when sensory stimuli are consciously perceived. Proc Natl Acad Sci U S A 112:

E2083-2092.

43. Ledberg A, Montagnini A, Coppola R, Bressler SL (2012) Reduced variability of ongoing and

evoked cortical activity leads to improved behavioral performance. PLoS One 7: e43166.

44. Arazi A, Censor N, Dinstein I (2017) Neural Variability Quenching Predicts Individual

Perceptual Abilities. J Neurosci 37: 97-109.

45. Saberi-Moghadam S, Ferrari-Toniolo S, Ferraina S, Caminiti R, Battaglia-Mayer A (2016)

Modulation of Neural Variability in Premotor, Motor, and Posterior Parietal Cortex during

Change of Motor Intention. J Neurosci 36: 4614-4623.

46. Churchland MM, Yu BM, Ryu SI, Santhanam G, Shenoy KV (2006) Neural variability in

premotor cortex provides a signature of motor preparation. J Neurosci 26: 3697-3712.

Legends

Fig 1. Predicting aspects of feeding behavior. **A.** Temporal dynamics of feeding behavior characterized on a population level across the four groups: baseline binge-like feeding of palatable chow (Base); binge-like feeding of palatable chow after 24-hours of food deprivation (Dep24) and 48-hours of food deprivation (Dep48); and limited access to house chow after 24-hours of food deprivation (Chow). Session lengths were normalized and the percent of animals feeding was smoothed for visualization. **B.** Kilocalories (kCal) consumed across conditions. More calories were consumed in Dep48 ($n = 8$) than Base ($n = 12$), and in both Dep24 ($n = 12$) and Dep48 than Chow ($n = 8$). Red bar indicates group average. * p < 0.05, ** p < 0.01 The change in kCal consumed were also used to calculate change in voracity (Figure 1-1A) which was then used to identify features potentially contaminated by chewing artifact (Figure 1-1B). **C.** Overview of analysis flow. Recordings were broken into non-overlapping 5 second bins and were assigned to one of 4 categories: not-feeding, rest, feeding, and pre-feeding. Power and coherence were calculated from each bin and averaged together according to category. Average brain activity of each animal during feeding was then normalized by activity during rest and used as predictor variables with behavioral metrics from that animal used as outcome variables. Outcome variables were then permuted to create distributions of 'by-chance' performances. **D-E.** Performance of models in predicting behavioral metrics; black distributions are performances of models using actual outcome variable assignment and white distributions are performances of models using permuted outcome variables. Distribution statistics reported as mean±95% confidence interval and effect size between Actual and Permuted given as Cohen's *d*. **D.** Mean absolute error (MAE) of predicting baseline food consumption in grams (gm). Actual = 2.6±0.08 gm; Permuted = 3.2±0.05 gm; $d = 0.43$. **E.** MAE of predicting percent change (%) in food consumption in Dep24 and Dep48 compared to Base (%): Actual = 0.8±0.01%; Permuted = 1.2±0.01%; $d = 1.1$. **F.** Percent accuracy (%) in predicting if house chow or palatable food was being consumed: Actual: 59±1%; Permuted: 50±1%; $d = 0.52$.

Fig 2. Classifying imminent feeding from other behavior with VS oscillations. **A.** Overview of

analysis flow. Data was binned and power and coherence extracted as in Figure 1. Orange box:

Eighty percent of all pre-feeding bins immediately before feeding bins and all other bins outside

of feeding (not-feeding and rest) are used for model training and the other 20% are used for

testing. Using the same data, the assignment of category to predictor variables is permuted and

trained on 80% of the data and tested on the left out 20%. This analysis produces two receiver

operator (ROC) curves representing the performance of models built from actual and permuted

data. To build rare event detectors (feeding is only ~18% of the data) the adaptive synthetic

sampling approach for imbalanced learning was found to be the best option (Figure 2-1A-B). To

be able to compare across models it was also necessary to determine the number of samples

were required to achieve stable model performance (Figure 2-1A-D). **B.** Average performance

of differentiating pre-feeding immediately before feeding begins and bins outside of feeding (not-

feeding and rest); performance distribution statistics reported as AUC mean ± 95% confidence

interval and the effect size between Actual and Permuted given as Cohen's *d*: Actual =

0.81±0.03; Permuted = 0.55±0.06; *d* = 2.68. **C.** Average areas under the ROC curves ($\overline{AUC}$)

obtained for 20 iterations of model building using models built from the pre-feeding bins

immediately preceding feeding and tested on all other pre-feeding bins grouped by amount of

time before feeding up to bins centered 42.5 seconds before feeding. **D.** Percent of pre-feeding

data which overlaps with approach behavior; pre-feeding bins centered up to 12.5 seconds

before feeding have at most 30% overlap with approach behavior. **E-F.** Normalized

representative LFP features plotted through time around feeding. Features were normalized by

either total power or by average coherence of the channel(s) of interest and averaged across all

bins and animals around the beginning and end of feeding epochs. Shading indicates ±1

standard deviation. Black traces represent averages before and after feeding and blue traces

represent averages during feeding. Dashed blue and solid black lines indicate average feature

activity for either feeding bins or all other bins including those outside of these plots. **E.** Core left

core right high gamma coherence increases during feeding. **F.** Shell left high gamma power

decreases during feeding. Although both **E** and **F** exhibit a mean shift, a decrease in feature

variance around feeding was also found (Figure 2-2).

Fig 3. Number of individuals needed to build models. **A.** Schema of factors influencing model

complexity and affected facets of model performance. Dashed outline indicates that a given

factor is being manipulated in current analysis and that the performance is being measured

accordingly. **B.** (Inset) The number of individuals and performance stability across individuals is

assessed by comparing the average performance of population models (i) built using 80% of all

animals' data and tested on the remaining 20% (All = 0.87±0.01; d = 3.27), using a leave-one

out (LOO = 0.78±0.06; d = 3.13) approach, and using permuted data in a leave-one out

approach (Permuted = 0.51±0.02) to the average performance of individual models (ii) built from

80% of each animals' data and testing on that animals' left out 20% (Self = 0.89±0.06; d = 3.13)

alongside permuted individual models (Permuted = 0.52±0.02). (iii) The subtraction of individual

model performance on classifying the left out data of that individual from the performance of

population models on the same data shows that individual models almost always outperform

population models, using both All and LOO datasets. **C.** Average performance of models built

from all possible combinations of including 1 to 12 individuals and tested on population data.

Circle indicates mean and vertical bar indicates 95% confidence interval.

Fig 4. Number of LFP features needed to classify feeding. **A.** Average performance of models

built and tested on population baseline data as the number of features used is manipulated

(Inset): single features (Monad), two features (Dyad), and three features (Triad), using lasso

(Lasso), and all 58 features (Logistic).The top dyad and triad were not composed of the top two

and three monad models, suggestive of the redundancy of LFP features (Figure 4-1)**.** Average

performance of all population baseline Monads, Dyads, Triads, and full Logistic across

conditions (Inset). Averages represented by circles and 95% confidence intervals by vertical

bars.

Fig 5. Performance of Population (black) and Individual (grey) models built from Baseline (**A**) and all condition (**B**) data and tested across states. **A.** Testing performance of population and individual models built from baseline data on all conditions (Inset). Population models built from Base do better than individual models when predicting behavior during any other condition than Base. **B.** Testing performance of population and individual models built from all conditions on all conditions (Inset). When models are built from all conditions, individual models do better than population models across conditions. * $p < 0.05$, ** $p < 0.01$, *** $p < 0.001$. Averages represented by circles and 95% confidence intervals by vertical bars.

Fig 6. Manipulating all number of features and using all conditions to find simplest individualized models (Inset) and using the full 58 feature logistic regression (Log) as the performance to match. For predicting behavior at Base (**A**) and Chow (**D**) two features are sufficient to achieve maximal performance. For Dep24 (**B**) three features are sufficient and for Dep48 (**C**) Lasso is required. **A.** Only Monads have significantly lower performance than the full Log, $t(14) = 4.04$, $p = .019$. **B.** Monads, $t(14) = 5.07$, $p = .0027$, and Dyads, $t(14) = 3.58$, $p = 0.049$, $p =$ have significantly lower performance than Log. **C.** Monads, $t(14) = 3.85$, $p = .028$, Dyads, $t(14) = 6.12$, $p = .00042$, and Triads, $t(14) = 5.51$, $p = .0012$, have lower performance than Log. **D.** Only Monads have significantly lower performance than Log, $t(14) = 3.70$, $p = 0=.038$. * $p < .05$, ** $p < .01$, and *** $p < .001$. Averages represented by circles and 95% confidence intervals by vertical bars.

Table 1. Appearance of frequency ranges in top-tier models (models that are not significantly worse than the top performer). There are 2 Monads, 8 Dyads, and 32 Triads within the top-tier (Table 1-1). Percentages of dyads and triads do not add to 100% since each model can contain more than one frequency range.

Fig S1. Features potentially contaminated by chewing noise **A.** Distribution of percent changes in voracity from baseline to food deprived conditions (Dep24 and Dep 48). **B.** Regression

between percent change in shell left core left theta coherence and percent change in voracity

from baseline to food deprived conditions; $p < 0.01$; $R^2 = 0.3$.

Fig S2. Learning curves used to determine minimum number of trials required to make models

whose performance stability are comparable. Circles indicate average AUC and vertical bars

represent 95% confidence intervals. Grey boxes indicate at which trial number performance

becomes insignificantly different from performance of models with most data. **A.** Testing

population models using ADSYN imputation and between 6 and 500 trials per animal; 150 per

animal (1800 total) are needed to achieve performance of models using all 500 per animal

(6000 total). **B.** Testing population models using weighted outcome variables and between 6

and 500 trials per animal; 350 trials per animal (4200 total) would be needed to match

performance of full models. **C.** Testing individual models (grey lines) using between 30 and 500

trials; the most any individual needed was 350 trials to match the performance of models made

with all 500 trials. **D.** Testing pre-feeding models using between 4 and 350 trials each; 13 trials

per animal were needed to match the performance of 350 trials per animal.

Fig S3. Monad feature performance with features used for top performing Dyad and Triad

indicated and features with 100% survival in the top performing Lasso models highlighted in red.

Average AUC indicated by a circle and 95% confidence interval by a vertical bar.

Fig S4. Shell right low gamma power exhibits a marked decrease in variation during feeding.

Power was normalized by total power of shell right and averaged across all trials and animals

around the beginning and end of feeding epochs. Shading indicates ±1 standard deviation.

Black traces represent averages before and after feeding and blue traces represent averages

during feeding. Dashed blue and solid black lines indicate average feature activity for either

feeding trials or all other trials outside of these plots.

Table S1. Top-tier monads, dyads, and triads with features and performances (area under the

curve, AUC). Locations: Sell left (SL), shell right (SR), core left (CL), core right (CR).

Frequencies: delta (d), theta (t), alpha (a), beta (b), low gamma (lg), and high gamma (hg).

Power features have one location and frequency (e.g. shell right alpha power is SRa) and

coherence have two locations and one frequency (e.g. high gamma coherence between shell

left and core right is SLCRhg). Feature order (Feature 1 vs. Feature 2) is not important.