# Data-driven approaches for Tau-PET imaging biomarkers in Alzheimer's disease

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## ABSTRACT

Previous positron emission tomography (PET) studies have quantified filamentous tau pathology using regions-of-interest (ROIs) based on observations of the topographical distribution of neurofibrillary tangles in post-mortem tissue. However, such approaches may not take full advantage of information contained in neuroimaging data. The present study employs an unsupervised data-driven method to identify spatial patterns of tau-PET distribution, and to compare these patterns to previously published "pathology-driven" ROIs. Tau-PET patterns were identified from a discovery sample comprised of 123 normal controls and patients with mild cognitive impairment or Alzheimer's disease (AD) dementia from the Swedish BioFINDER cohort, who underwent [18F]AV1451 PET scanning. Associations with cognition were tested in a separate sample of 90 individuals from ADNI. BioFINDER [18F]AV1451 images were entered into a robust voxelwise stable clustering algorithm, which resulted in five clusters. Mean [18F]AV1451 uptake in the data-driven clusters, and in 35 previously published pathology-driven ROIs, was extracted from ADNI [18F]AV1451 scans. We performed linear models comparing [18F]AV1451 signal across all 40 ROIs to several tests of global cognition, adjusting for age, sex and education. Two data-driven ROIs consistently demonstrated the strongest or near-strongest effect sizes across all cognitive tests. Inputting all regions plus demographics into a feature selection routine resulted in selection of two ROIs (one data-driven, one pathology-driven) and education, which together explained 28% of the variance of a global cognitive composite score. Our findings suggest that [18F]AV1451-PET data naturally clusters into spatial patterns that are biologically meaningful and that may offer advantages as clinical tools.

## 1. INTRODUCTION

Alzheimer's disease (AD) is neuropathologically defined by the presence of widespread extracellular plaques containing amyloid-β and intracellular neurofibrillary tangles consisting of aggregated tau proteins [Braak and Braak, 1991; Masters et al., 1985]. While amyloid-β may be present decades prior to symptom onset [Jansen et al., 2015], the presence of neocortical tau is temporally more closely related to current cognitive status and degree of neurodegeneration, as convincingly demonstrated by studies utilizing post-mortem tissue, animal models, cerebrospinal fluid and, more recently, the positron emission tomography (PET) tracer [$^{18}$F]AV1451 [Arriagada et al., 1992; Bejanin et al., 2017; Cho et al., 2017; Nelson P. T. et al, 2013; Ossenkoppele et al., 2016; Van Rossum et al., 2012]. [$^{18}$F]AV1451 binds paired helical filaments of tau with high affinity and selectivity [Chien et al., 2013; Lowe et al., 2016; Marquié et al., 2015; Marquié et al., 2017; Xia et al., 2013], and can be used to investigate the distribution of tau pathology in the living human brain. Several studies have shown strong spatial resemblance between *in vivo* tau PET patterns and neuropathological staging of neurofibrillary tangles as proposed by Braak and Braak [Cho et al., 2016; Schöll et al., 2016; Schwarz et al., 2016], reflecting prototypical progression from (trans)entorhinal (stage I/II) to limbic (stage III/IV) to isocortical (stage V/VI) regions [Braak and Braak, 1991]. Furthermore, regional [$^{18}$F]AV1451 retention co-localizes with sites of brain atrophy or hypometabolism [Ossenkoppele et al., 2016; Xia et al., 2017] and has been associated with impairments in specific cognitive domains [Bejanin et al., 2017; Cho et al., 2017; Ossenkoppele et al., 2016].

Given this strong regional specificity of tau pathology, it is important to consider

how regions-of-interest (ROIs) are defined, as they could potentially impact study

outcomes. To date, most studies employing tau-PET tracers involved ROIs constructed

based on neuropathological studies. For example, some studies mimicked the Braak

stages *in* vivo [Cho et al., 2016; Schöll et al., 2016; Schwarz et al., 2016], while others

selected specific regions reflecting early (e.g. entorhinal cortex) or more advanced (e.g.

inferior temporal cortex) disease stages [Johnson et al., 2016]. These approaches have

several advantages as they are supported by fundamental research and enhance

generalizability across studies. However, compared to neuroimaging, neuropathological

data typically include only a few slices in a constrained number of brain regions, and

brain tissue is affected by death [Scheltens and Rockwood, 2011]. Additionally, tau PET

signal does not equal presence of tau pathology. There are several sources of

[$^{18}$F]AV1451 signal and noise, including target binding, off-target binding (e.g.

Monamine oxidase, neuromelanin, vascular lesions, iron), non-specific binding and

imaging related noise (e.g. partial volume effects) [Choi et al., 2017; Harada et al., 2017;

Ikonomovic et al.,; Lockhart et al., 2017; Lowe et al., 2016; Marquié et al., 2015; Ng et

al., 2017; Schöll et al., 2016]. An alternative approach could therefore be to select ROIs

based on data-driven approaches [Dickerson et al., 2011; Landau et al., 2011; Pankov et

al., 2016], thereby taking full advantage of the abundance of information contained in

neuroimaging data, but also accounting the idiosyncrasies of PET imaging data.

In light of ongoing efforts to define appropriate ROIs and determine tau PET-

positivity, it is important to compare data-driven approaches (agnostic, "where is the

tau?") with theory-derived ROIs based on post-mortem studies (directed, "is the tau

here?"). In the present study, we applied an unsupervised algorithm to identify clusters of

[$^{18}$F]AV1451 signal. We then compared the spatial patterns of these clusters with

neuropathologically derived ROIs described in previous publications. Finally, we tested

which ROI best correlated with global cognition in an independent cohort of cognitively

normal, mild cognitive impairment and AD dementia subjects. We hypothesized that our

data-driven approach would corroborate neuropathological findings, but would also

present novel information leading to enhanced associations with cognition.

**2. MATERIALS AND METHODS**

**2.1 Participants**

Two separate cohorts were included in this study. Participants from the Swedish

BioFINDER study were used to perform clustering analysis on [$^{18}$F]AV1451 data,

whereas participants from the Alzheimer's Disease Neuroimaging Initiative (ADNI) were

used to test associations between the clustering-derived ROIs and cognition.

Demographic, clinical and biomarker information for both cohorts are presented in Table

1.

The BioFINDER cohort is a multi-site study designed for the purpose of

developing biomarkers for neurodegenerative diseases. More information can be found at

http://biofinder.se. Study participants included 55 subjects with normal cognition, 21 with

(MCI), and 47 with Alzheimer's dementia, who had complete MRI and [$^{18}$F]AV1451

PET data (Table 1). Patients with MCI were referred to a memory clinic and

demonstrated objective cognitive impairment that could not be explained by another

condition. AD dementia patients met criteria for the DSM-V [American Psychiatric

Association, 2013] and NINCDS-ADRDA [McKhann et al., 2011] for probable AD,

established by clinicians blinded to PET data. To optimize overlap with the ADNI cohort,

dementia patients were only included if they presented with an amnestic-predominant

phenotype. Both dementia and MCI patients were only included in this study if they

demonstrated abnormal Aβ1-42 levels in the CSF (INNOTEST, cut-off: 650 ng/l;

Palmqvist *et al.*, 2015). The sample of controls selected for [$^{18}$F]AV1451 scanning was

intentionally enriched for β-amyloid positivity to include people in the preclinical stage

of AD (see Table 1). PET imaging for the study was approved by the Swedish Medicines

and Products Agency and the local Radiation Safety Committee at Skåne University

Hospital, Sweden. All participants provided written informed consent according to the

Declaration of Helsinki, and ethical approval was given by the Ethics Committee of Lund

University, Lund, Sweden.

ADNI is a multi-site open source dataset designed to accelerate the discovery of

biomarkers to identify and track AD pathology [Weiner et al., 2012]. The current study

included all ADNI individuals with complete [$^{18}$F]AV1451 scans that were available in

November, 2016. This included 43 cognitively normal elderly controls, 37 patients with

MCI, and 10 patients with a recent diagnosis of Alzheimer's dementia (Table 1).

In addition to imaging data, age, sex, education, diagnosis, amyloid-β status on

[$^{18}$F]florbetapir PET [Landau et al., 2013], and scores from six tests measuring global

cognition or activities of daily living were downloaded from the ADNI-LONI website

(adni.loni.usc.edu). The cognitive tests were as follows: Mini-Mental State Examination

(MMSE) [Folstein et al., 1975]; Clinical Dementia Rating Sum of Boxes (CDRSB)

[Hughes et al., 1982]; Alzheimer's disease Assessment Scale 11 (ADAS11) [Rosen et al.,

1984] and 13 (ADAS13) [Mohs et al., 1997]; Everyday Cognition (ECog) [Farias et al.,

2008]; Functional Activities Questionnaire (FAQ) [Pfeffer et al., 1982].

**2.2 Imaging**

[$^{18}$F]AV1451 images were processed using separate but nearly identical pipelines across

the two cohorts. Acquisition and processing procedures for [$^{18}$F]AV1451 processing in

the BioFINDER cohort has been described elsewhere [Hansson et al., 2017]. Scans were

reconstructed into 5-min frames and motion corrected using AFNI's 3dvolreg

https://afni.nimh.nih.gov/. Mean [$^{18}$F]AV1451 images were created over a time-window

of 80-100 minutes post-injection, and these images were coregistered to each subject's

T1 image in native space. Mean images were then intensity normalized using a complete

cerebellar gray reference region to create standard uptake value ratio (SUVR) images.

Coregistered MRI images were normalized to the MNI-ICBM152 template using

Advanced Normalization Tools (https://stnava.github.io/ANTs/) and the transformation

parameters were applied to the SUVR images. Finally, SUVR images were smoothed

with an 8mm FWHM Gaussian filter.

173           For the ADNI cohort, mean 80-100 min [$^{18}$F]AV1451 images, as well as

MPRAGE images closest to [$^{18}$F]AV1451 scans, were downloaded from the ADNI-LONI

website. Details on acquisition procedures for these [$^{18}$F]AV1451 and MRI images can be

found elsewhere (http://adni.loni.usc.edu/methods/documents/). [$^{18}$F]AV1451 images

were processed in accordance to procedures described in [Schöll et al., 2016]. Briefly, T1

images were processed using Freesurfer v5.3 and [$^{18}$F]AV1451 images were coregistered

to native T1s using Statistical Parametric Mapping 12 (www.fil.ion.ucl.ac.uk/spm/).

SUVR images were created using a cerebellar gray reference region and images were

normalized to MNI space using the parameters from the coregistered T1. Figure 1 shows

mean [18F]AV1451 SUVR images stratified by diagnosis and amyloid status for each

cohort.

**2.3 Clustering of [18F]AV1451 data**

Cross-subject [18F]AV1451-PET covariance networks were derived from all 123

BioFINDER [18F]AV1451 images using an open-source unsupervised consensus-

clustering algorithm called Bootstrap Analysis of Stable Clusters (BASC; Figure 2)

[Bellec et al., 2010]. The algorithm was adapted to 3D [18F]AV1451 data by stacking all

123 BioFINDER [18F]AV1451 images along a fourth (subject) dimension, creating a

single 4D image to be submitted as input. BASC first reduces the dimensions of the data

with a previously described region-growing algorithm [Bellec et al., 2006], which was set

to extract spatially constrained atoms (small regions of redundant signal) with a size

threshold of 1000mm$^3$. In order to reduce computational demands, the Desikan-Killainy

atlas [Desikan et al., 2006] was used as a prior for region constraint, and the data was

masked with a liberal gray matter mask, which included the subcortex but had the

cerebellum manually removed (since this was used as the reference region for

[18F]AV1451 images). The region-growing algorithm resulted in a total of 730 atoms,

which were included in the BASC algorithm. BASC next performs recursive k-means

clustering on bootstrapped samples of the input data. After each clustering iteration,

information about cluster membership is stored as a binarized adjacency matrix. The

adjacency matrices are averaged resulting in a stability matrix representing probabilities

203 of each pair of atoms clustering together (Figure 2). Finally, hierarchical agglomerative

204 clustering with Ward criterion is applied to the stability matrix, resulting in the final

205 clustering solution. The process is repeated over several clustering solutions (k=1 - 50),

206 and the MSTEPs method [Bellec, 2013] was implemented to find the most stable

207 clustering solutions at different resolutions. In the interest of multiple comparisons, and

208 similarity to Braak neuropathological staging (i.e. six ROIs), we chose the lowest

209 resolution solution for subsequent analysis. Note that no size constraints were imposed on

210 clustering solutions. Voxels were only included in a cluster when cluster probability

211 membership exceeded 0.5 (BASC default setting), eliminating unstable voxels from

212 analysis [Bellec et al., 2010; Garcia-Garcia et al., 2017]. After determining clusters in the

213 BIOFINDER cohort, we extracted the (size-weighted) average [$^{18}$F]AV1451 SUVR for

214 each cluster from all ADNI subjects, and these values were used for subsequent analysis

215 investigating associations with cognition.

216   BASC was chosen over other clustering algorithms because its bootstrapping

217 feature offers two advantages in the context of this study. First, the stochastic nature of

218 many clustering algorithms tends to lead to different solutions depending on their

219 initialization state, whereas BASC performs clustering on a stability matrix generated

220 from many solutions (and thus many initializations). This leads to greater reproducibility

221 in the clustering solutions generated by BASC. Second, because the initial set of

222 clustering analyses is performed on bootstrap samples of the input data, the final solution

223 is less dependent on the clinical composition of the input data.

225 **2.4 Definition of Braak stage ROIs described in other studies**

A number of studies have created ROIs mirroring the Braak stages described from

pathological studies. To test the utility of our data-driven ROIs vis-à-vis those defined in

correspondence to the pathological literature, we recreated the Braak ROIs described in

three different studies [Cho et al., 2016; Schöll et al., 2016; Schwarz et al., 2016]. Schöll,

Lockhart et al. and Cho et al. were constructed using regions from the Desikan-Killainy

atlas, and we recreated these ROIs in direct correspondence to what has been reported in

these two studies. Schwarz et al. instead generated small ROIs designed to mirror the

slabs of cerebral cortex extracted during autopsy for Braak staging. These regions were

constructed with a script generously provided by the authors. For all analyses, Braak

ROIs were included both individually ("single") and cumulatively ("stage"). For

example, for Braak Stage III, one ROI was created containing all regions from Braak I,

II, and III included ("stage"), as well as a ROI created including only regions in Braak III

("single"). Finally, some studies have chosen to use only the bilateral inferior temporal

lobe from the Desikan-Killainy atlas to summarize global tau burden [Johnson et al.,

2016], so we included this region in subsequent analysis as well. Studies also frequently

used the bilateral entorhinal cortex from this atlas, and it should be noted that this region

is also included, namely as Stage I from Cho et al. and Schöll, Lockhart et al. Size-

weighted average [$^{18}$F]AV1451 SUVR was extracted for each ROI (35 in total) for each

subject.

**2.5 Similarity between data-driven clusters, anatomical ROIs and Braak**

**Stage ROIs**

We compiled descriptive information about the similarity between our cluster-

derived ROIs and the Braak ROIs from the literature. For comparisons to regions from

Schöll, Lockhart et al. and Cho et al., we used normalized mutual information. Due to the

small size of the Schwarz et al. regions, comparisons involved measuring the percentage

of each Schwarz ROI falling inside of each cluster-derived ROI.

**2.6 Statistical Analysis**

In order to test the utility of our data-driven covariance networks, we performed

linear models between these covariance networks and the scores from six different

available test scores assessing global cognition and function (see Table 2). In addition,

the scores were summarized using Principal Components Analysis (PCA) using Singular

Value Decomposition. The PCA was fit to data from the six cognitive test scores, which

were scaled to a 0 mean with unit variance. The first component explained 72% of the

total model variance, and was used to transform the cognitive data into a single Global

Cognition composite score. For each of the cognitive tests, as well as the composite

score, separate general linear models for each ROI (40 in total; our five data-driven

clusters and 35 ROIs from the literature) were constructed with cognitive test score as the

dependent variable and age, sex and education as covariates. Tests surviving Bonferroni

correction for multiple comparisons are reported.

In order to identify a sparse set of non-redundant covariates that best describe the

global cognitive data in ADNI, we submitted all 40 tau ROIs plus age, sex and education

to a Least Absolute Shrinkage and Selection Operator (Lasso) regression-based feature

selection routine. The Lasso uses L1 regularization (coordinate descent) to penalize

regression coefficients based on their maximum likelihood estimates, and is therefore an

optimal approach to select a small number of variables from a large number of collinear

covariates. In the current implementation, the degree of penalization is optimized using

10-fold cross-validation. All tau ROIs and demographics were scaled to be mean-

centered with unit variance, and entered into the Lasso regression model with the Global

Cognition composite score as the dependent variable. Features selected by the Lasso

(absolute beta > 0.25) were entered together into a general linear model (GLM) with

MMSE as the dependent variable. Additionally, to ensure our results were representative

of global cognition and not specific to the composite score, the fitted values from this

GLM were used to predict scores of each of the six cognitive tests. Finally, the Lasso was

repeated separately for each of the individual test as well.

With the exception of BASC, all statistics were implemented using the pandas,

numpy, scipy and scikit-learn [Pedregosa et al., 2012] packages in Python 3.5.2

(https://www.python.org/).

**3. RESULTS**

**3.1 Participant Characteristics**

Table 1 contains demographic information, MMSE scores and amyloid positivity

rates for both the ADNI and BioFINDER sample. The sample used for clustering

(BioFINDER) demonstrated important differences compared to the sample used for

testing (ADNI). BioFINDER subjects were less highly educated across the whole sample,

and BioFINDER controls were on average older than ADNI controls. Additionally, the

BioFINDER sample demonstrated lower MMSE scores across the whole sample

compared to ADNI, including within MCI and dementia groups. Finally, 45% of ADNI

subjects were amyloid-positive vs. 73% of BioFINDER subjects, which was primarily

related to the fact that only amyloid positive MCI patients were included in the

BioFINDER sample.

**3.2 Data-driven Tau-PET covariance networks**

123 BioFINDER [$^{18}$F]AV1451 scans were entered into an advanced clustering

algorithm in order to identify networks of regional [$^{18}$F]AV1451 signal covariance across

subjects. The M-STEPS algorithm identified five-, nine- and 32-cluster solutions as

optimal solutions. For the purposes of comparing with Braak stage ROIs, we chose the

lowest-resolution solution (n=5) for subsequent analyses, visualized in Figure 2. The

clusters were interpreted and named as follows: "1: Subcortical", "2: Frontal", "3:

Medial/Anterior/Inferior Temporal", "4: Temporo-parietal" and "5: Unimodal Sensory".

Cluster 3 bore resemblance to regions often involved in early tau aggregation and atrophy

[Braak and Braak, 1991], while Cluster 4 also appeared similar to regions commonly

associated with neurodegeneration in AD [Dickerson et al., 2011; Landau et al., 2011].

Of note, the hippocampus was largely unrepresented in any of the cluster-cores, though

some voxels in the head of the hippocampus were included in Cluster 3, and a few

distributed voxels were included in Cluster 1 (Subcortex). However, using a winner-

takes-all clustering approach, the majority the hippocampal voxels clustered with other

subcortical and periventricular regions.

**3.3 Similarity to Braak ROIs**

Descriptive metrics were used to quantify the spatial similarity between the data-driven

covariance networks and the Braak Stage ROIs introduced in the literature (Figure 3).

Cluster 5 ("Unimodal Sensory") demonstrated a high degree of overlap with Braak Stage

VI across all region sets. Spatial similarity was also evident between Cluster 3

("Medial/Anterior/Inferior Temporal") and Stage I-IV from Cho et al., and this cluster

almost completely circumscribed Stages I-III from Schwarz et al. Cluster 1 ("Subcortex")

was most similar to Schöll, Lockhart et al. Stage II, due in part to its inclusion of the

hippocampus. Little spatial similarity was evident between Cluster 2 ("Frontal") and any

of the Braak Stage ROIs, though some similarity was seen with the Stage V region from

Schöll, Lockhart et al. and Cho et al. due to their inclusion of many frontal lobe

structures. Similarly, Cluster 4 ("Temporo-parietal") did not demonstrate strong spatial

similarity to any of the Braak ROIs, though it did partially overlap with the Braak Stage

VI and Stage V regions from Schwarz et al.

**3.4 Associations with global cognition in ADNI**

332           General linear models were run in the ADNI dataset assessing associations

separately between each of 40 tau ROIs (our five data-driven clusters established in the

BioFINDER study, and 35 ROIs from the literature) and a Global Cognitive composite

score, controlling for age, sex and education (Figure 4). AV1451 signal in several ROIs

demonstrated strong associations with global cognition, though only the data-driven

Cluster 4 ("Temporo-parietal"; $\beta$ = -3.24 [SE=0.91], t = -3.43, p<0.001) survived

multiple comparisons.

To ensure our results were not specific to the Global Cognition composite score,

we repeated this analysis using the six individual measures of global cognition and

function that composed the composite score (Table S1). The data-driven Cluster 4

("Temporo-parietal") described global cognition better than all other ROIs using four of

the six cognitive measures, and was in the top five for all of them. Across all cognitive

measures, Clusters 4 and 3 ("Medial/anterior/inferior temporal") ranked best and second

best, respectively, at describing global cognitive data (Figure 5). Notably, the Schwarz

Stage I ROI also performed well across cognitive measures, except for the MMSE.

**3.5 Identifying a combinatorial tau-PET biomarker for cognition**

Next, all tau ROIs were entered into a Lasso regression model in order to identify

a sparse set of covariates that best describe global cognitive data (Figure 6). The optimal

penalization value was defined through cross-validation as 0.019. The Lasso reduced all

coefficients except Cluster 4 ("Temporo-parietal"), Braak Stage VI from Schwarz et al.,

and education. These three variables were entered together into a general linear model,

and together explained a much greater proportion of variance in global cognitive data

($r^2[4:81] = 0.28$, $p<0.0001$; Figure 5) compared to the individual effect sizes of each

covariate (highest $r^2 = 0.12$). The earlier negative association between Cluster 4 and

Global Cognition was strengthened (t=-4.98, p<0.001), although positive associations

were seen for the other two covariates (Schwarz Single 6: t = 3.61, p = 0.001; Education:

t = 2.53, p = 0.013). In addition, the fitted values of this GLM explained 18.7 – 26.2% of

the variance in the six individual cognitive tests composing the composite score (all p

<0.001), indicating the model generalizes well to individual cognitive tests (Table S2).

Finally, the Lasso feature selection analysis was repeated for the six individual tests of

global cognition. The data-driven Cluster 4 was selected across all six analyses, and was

the only ROI selected for two analyses (Table S3).

**4. DISCUSSION**

In the present study, we applied an advanced unsupervised algorithm to identify

clusters of [$^{18}$F]AV1451 signal in 123 subjects ranging from cognitively normal to AD

dementia in the Swedish BioFINDER study. Our approach yielded clusters in the

temporoparietal, medial/inferior/anterior temporal, unimodal sensory and frontal cortex,

as well as the subcortex. In an independent sample of 90 subjects (ADNI), we performed

general linear models between tests of global cognition and each [$^{18}$F]AV1451 cluster,

adjusting for age, sex and education. In addition, we ran similar models using 35

neuropathologically derived ROIs from previous publications [Cho et al., 2016; Johnson

et al., 2016; Schöll et al., 2016; Schwarz et al., 2016]. Several ROIs exhibited strong

relationships with cognition, though certain data-driven clusters (temporoparietal and

medial/inferior/anterior temporal cortex) appeared to perform slightly but consistently

better than other ROIs in ADNI. Supporting this notion, the temporoparietal data-driven

cluster was among the three most important features (identified by a Lasso regression

model) for predicting global cognition scores. Unsupervised clustering of [$^{18}$F]AV1451

PET data thus revealed the data to self-assemble into ROIs resembling well described

vulnerable regions in AD, some of which actually enhanced description of cognitive data

in an independent dataset. This suggests that data-driven approaches to delineate ROIs

may improve clinical utility of [$^{18}$F]AV1451 PET data.

The tau-PET covariance networks derived from our clustering approach exhibited

a fair degree of overlap with Braak ROIs derived from autopsy studies, thereby

demonstrating biological relevance. Particularly, Cluster 3 ("Medial/Anterior/Inferior

Temporal") was reminiscent of regions involved in early tau accumulation, whereas

Cluster 5 ("Unimodal Sensory") demonstrated a high degree of similarity to regions

involved only in the latest stages of AD. In contrast, Cluster 4 ("Temporo-parietal") did

not strongly resemble any of the Braak regions, while its pattern, together with the pattern

of cluster 3, spatially overlapped with cortical regions most vulnerable to

neurodegeneration in AD [Dickerson et al., 2011; Landau et al., 2011]. Furthermore,

signal in the hippocampus was heterogenous, adding additional evidence that

$[^{18}F]$AV1451 signal in this structure should be interpreted with caution [Cho et al., 2016]

[Choi et al., 2017; Ikonomovic et al.,]. Similarly, our data-driven approach suggested that

most (but not all) frontal lobe structures exhibited $[^{18}F]$AV1451 signal patterns unique to

the rest of the cortex. This is notable considering the original Braak Stage V aggregates

frontal lobe structures with many of the temporo-parietal structures captured in our

Cluster 4. Part of the successful description of cognitive data by the data-driven ROI may

be due to its isolation from many of these frontal lobe structures, which may be

contributing signal less informative to AD progression, particularly in early disease

stages. Finally, our data-driven ROIs provide information that may reconcile some

differences between existing Braak ROIs. For example, in our study, $[^{18}F]$AV1451 signal

in the putamen and insula covaried with other regions involved in early tau accumulation,

which was similar to the ROIs described by Schöll, Lockhart et al., but not Cho et al. (see

Table S4 for a summary).

Despite the clusters being derived from a sample with several important and

disease-relevant differences compared to the testing sample, these data-driven ROIs

described global cognitive data slightly better than regions derived from autopsy studies.

While the improvement over the other regions was subtle, the increasing movement

toward the development of biomarkers demands optimization of ROIs to summarize

$[^{18}F]$AV1451 signal [Frisoni et al., 2017; Maass et al., 2017; Mishra et al., 2017]. As

such, even small improvements are important for studies assessing more subtle effects of

cortical tau accumulation and studies seeking optimal biomarkers for multimodal

classification or disease progression [Ota et al., 2015]. The improvement observed is

likely due to the data-driven nature of the method used for derivation of the clusters.

$[^{18}F]$AV1451 may be binding to several off-target agents, such as (neuro)melanin, iron,

vascular pathology and MAO-A/B [Choi et al., 2017; Lowe et al., 2016; Marquié et al.,

2015; Ng et al., 2017], and as such, $[^{18}F]$AV1451 signal is likely a mix of true tau

pathology and other off-target and non-specific signals. Deriving the clusters from a

sample representing a wide breadth of disease stages and additionally including subjects

unlikely to have significant cortical tau pathology enhances the likelihood of isolating

true tau signal, which covaries strongly and in a regionally specific pattern across disease

stages. Additionally, deriving the clusters voxelwise allows freedom from anatomical

borders, which may impose unnecessary constraints irrelevant to the spread of tau.

Finally, despite its many limitations, multi-subject automatic whole-brain sampling is a

distinct advantage of $[^{18}F]$AV1451-PET over pathological studies. This advantage may

further enhance the efficacy of data-driven approaches to ROI generation, which evaluate

regions equally that may otherwise be overlooked.

The results of this study thus suggest a possible advantage of data-driven

approaches in evaluating [$^{18}$F]AV1451 PET data as a biomarker for AD. This study adds

to a rapidly growing body of data-driven [$^{18}$F]AV1451-PET studies that have helped to

characterize features of this tracer in the context of AD. Sepulcre and colleagues

employed a similar unsupervised clustering approach on a set of cognitively intact elderly

individuals, which, similar to our study, revealed [$^{18}$F]AV1451-PET covariance between

regions of early- and later- stage tau accumulation [Sepulcre et al., 2017]. This suggests

these patterns of signal covariance are stable even in the earliest disease stages, lending

credence to the use of data-driven biomarkers in multiple contexts. Meanwhile, Jones et

al. used a data-driven Independent Components Analysis approach to summarize

[$^{18}$F]AV1451 data [Jones et al., 2017]. While the authors concluded the resulting ROIs

represented functional brain networks, three of the ROIs bore a striking similarity to

those generated by our clustering approach. Our approach builds on these previous

studies by assessing relationships between data-driven ROIs and cognition, and by

comparing them with other existing ROIs. Maass et al. employed a series of *a priori* and

supervised data-driven methods to generate [$^{18}$F]AV1451 ROIs and found a relative

equivalence between these ROIs in their association with cognition and a number of other

disease markers [Maass et al., 2017]. However, consistent with our study, Maass et al.

found [$^{18}$F]AV1451 signal to covary most strongly within a specific set of AD

vulnerable-regions, and conclude that these regional measures may perform better than

whole-brain ROIs, particularly regarding associations with cognition.

We employed a widely used feature selection routine to identify those regions

most informative in describing association between [$^{18}$F]AV1451 signal and cognitive

data. The feature most strongly associated with global cognition was the data-driven

temporo-parietal cluster, which harbored a strong negative relationship when included

with the other selected features (p<0.001). The feature selection also resulted in the

selection of Schwarz et al. Stage VI and education, both of which associated positively

with MMSE in a general linear model. The finding of an association between education

and MMSE controlling for tau pathology is consistent with the concept of cognitive

reserve [Stern, 2012], and suggests that more highly educated subjects may experience

preserved cognition in the face of tau pathology [Hoenig et al., 2017]. While the selection

of Schwarz Stage VI is less obvious, possible explanations include partial volume effects

and age-related off-target or non-specific signal. Because very few ADNI subjects

demonstrate strong [$^{18}$F]AV1451 signal in this ROI, higher [$^{18}$F]AV1451 signal may be

related to the presence of more cortex (and thus more off-target or non-specific binding)

rather than increased tau pathology. Similarly, off-target [$^{18}$F]AV1451 signal in the

cortex and subcortex has been shown to increase with age [Choi et al., 2017; Schöll et al.,

2016; Smith et al., 2016], possibly representing binding to reactive astrocytes [Harada et

al., 2017] or iron deposits [Choi et al., 2017]. Since age was not selected by the Lasso and

therefore was not included in the multivariate model, this may explain the positive

association between these regions and global cognition when accounting for AV1451

signal in the temporoparietal region. However, the fact that these ROIs were selected

instead of age suggests they may carry additional cognition-relevant information, which

may demand further exploration. Regardless, the negative relationship between Cluster 4

("Temporo-parietal") and global cognition was substantially increased after regressing

out these other variables. This suggests that [$^{18}$F]AV1451-cognition relationships may be

enhanced by regressing out off-target or non-specific signal sources.

Our study comes with a number of limitations. First, there were several

differences in characteristics between the two samples. We decided to use the

BioFINDER cohort for clustering given the broad range of both [$^{18}$F]AV1451 uptake

(Figure 1) and cognitive scores (Table 1). As a consequence, validation of the clusters

was performed in subjects from the ADNI cohort with more restricted [$^{18}$F]AV1451

uptake and cognitive scores. On a related note, our cluster and results could be influenced

by the composition of our samples. However, voxels are only included in the clusters

derived for our analysis if the clustering occurs across >50% of bootstrap samples, so it is

unlikely that the clustering solution would be strongly driven by, for example, the high

proportion of late-stage (i.e. AD) subjects in the BioFINDER sample. Third, contrary to

other studies, we did not make an attempt to classify individuals according to stages of

tau pathology. Finally, we chose not to apply partial volume correction on our data.

Investigating the impact of such corrections is certainly important, but we were interested

in the natural behavior of tau-PET signal before any corrections.

In order to aid future studies, we have made the [$^{18}$F]AV1451 clusters from this

study available on FigShare (doi = 10.6084/m9.figshare.5758374).

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## Author Contributions

530 J.W.V. and R.O. conceptualized and designed the study. P.S., A.C.E., O.H. and R.O.

531 supervised the study. J.W.V., N.M., Y.I.M., T.O.S., M.S., P.B., O.H. and R.O. acquired,

532 processed and analyzed the data. J.W.V., W.F. and R.O. drafted the manuscript. All

533 authors provide critical or conceptual support and revised the manuscript.

## Potential Conflicts of Interest

American Psychiatric Association T (2013): Diagnostic and statistical manual of mental
disorders : DSM-5. Fifth edition. Arlington, VA : American Psychiatric Association,
[2013]. https://search.library.wisc.edu/catalog/9910187853902121.
Arriagada P V, Growdon JH, Hedleywhyte ET, Hyman BT (1992): Neurofibrillary
Tangles But Not Senile Plaques Parallel Duration and Severity of Alzheimers-
Disease. Neurology 42:631–639.
Bejanin A, Schonhaut DR, Joie R La, Kramer JH, Baker SL, Sosa N, Ayakta N, Cantwell
A, Janabi M, Lauriola M, O 'neil JP, Gorno-Tempini ML, Miller ZA, Rosen HJ,
Miller BL, Jagust WJ, Rabinovici GD (2017): Tau pathology and neurodegeneration
contribute to cognitive impairment in Alzheimer's disease. Brain:1–15.
https://watermark.silverchair.com/awx243.pdf?token=AQECAHi208BE49Ooan9kk
hW_Ercy7Dm3ZL_9Cf3qfKAc485ysgAAAecwggHjBgkqhkiG9w0BBwagggHUMI
IB0AIBADCCAckGCSqGSIb3DQEHATAeBglghkgBZQMEAS4wEQQM-
3OjnBKCYybpS8fEAgEQgIIBmpY9paVgrJr248NQgNg8LAw6UHj7Y8NzZqCqE
KPxMOE1DebS.
Bellec P (2013): Mining the hierarchy of resting-state brain networks: Selection of
representative clusters in a multiscale structure. Proc - 2013 3rd Int Work Pattern
Recognit Neuroimaging, PRNI 2013:54–57.
Bellec P, Perlbarg V, Jbabdi S, Pélégrini-Issac M, Anton JL, Doyon J, Benali H (2006):
Identification of large-scale networks in the brain using fMRI. Neuroimage
29:1231–1243.
Bellec P, Rosa-Neto P, Lyttelton OC, Benali H, Evans AC (2010): Multi-level bootstrap
analysis of stable clusters in resting-state fMRI. Neuroimage 51:1126–1139.
http://dx.doi.org/10.1016/j.neuroimage.2010.02.082.
Braak H, Braak E (1991): Neuropathological stageing of Alzheimer-related changes.
Acta Neuropathol 82:239–59. http://www.ncbi.nlm.nih.gov/pubmed/1759558.
Chien DT, Bahri S, Szardenings AK, Walsh JC, Mu F, Su M-Y, Shankle WR, Elizarov
A, Kolb HC (2013): Early Clinical PET Imaging Results with the Novel PHF-Tau
Radioligand [F-18]-T807. J Alzheimer's Dis 34:457–468.
Cho H, Choi JY, Hwang MS, Kim YJ, Lee HM, Lee HS, Lee JH, Ryu YH, Lee MS,
Lyoo CH (2016): In vivo cortical spreading pattern of tau and amyloid in the
Alzheimer's disease spectrum. Ann Neurol:1–12.
http://doi.wiley.com/10.1002/ana.24711.
Cho H, Choi JY, Lee SH, Lee JH, Choi YC, Ryu YH, Lee MS, Lyoo CH (2017):
Excessive tau accumulation in the parieto-occipital cortex characterizes early-onset
Alzheimer's disease. Neurobiol Aging 53:103–111.
http://dx.doi.org/10.1016/j.neurobiolaging.2017.01.024.
Choi JY, Cho H, Ahn SJ, Lee JH, Ryu YH, Lee MS, Lyoo CH (2017): "Off-Target" [18] F-
AV-1451 Binding in the Basal Ganglia Correlates with Age-Related Iron
Accumulation. J Nucl Med:jnumed.117.195248.
http://jnm.snmjournals.org/lookup/doi/10.2967/jnumed.117.195248.
Desikan RS, Ségonne F, Fischl B, Quinn BT, Dickerson BC, Blacker D, Buckner RL,
Dale AM, Maguire RP, Hyman BT, Albert MS, Killiany RJ (2006): An automated
labeling system for subdividing the human cerebral cortex on MRI scans into gyral
based regions of interest. Neuroimage 31:968–980.
Dickerson BC, Stoub TR, Shah RC, Sperling RA, Killiany RJ, Albert MS, Hyman BT,

Blacker D, Detoledo-Morrell L (2011): Alzheimer-signature MRI biomarker
predicts AD dementia in cognitively normal adults. Neurology 76:1395–1402.
Farias ST, Mungas D, Reed BR, Cahn-Weiner D, Jagust W, Baynes K, Decarli C (2008):
The measurement of everyday cognition (ECog): scale development and
psychometric properties. Neuropsychology 22:531–44.
http://www.ncbi.nlm.nih.gov/pubmed/18590364.
Folstein MF, Folstein SE, McHugh PR (1975): "Mini-mental state". A practical method
for grading the cognitive state of patients for the clinician. J Psychiatr Res 12:189–
98. http://dx.doi.org/10.1016/0022-3956(75)90026-6.
Frisoni GB, Boccardi M, Barkhof F, Blennow K, Cappa S, Chiotis K, Démonet J-F,
Garibotto V, Giannakopoulos P, Gietl A, Hansson O, Herholz K, Jack CR, Nobili F,
Nordberg A, Snyder HM, Ten Kate M, Varrone A, Albanese E, Becker S, Bossuyt
P, Carrillo MC, Cerami C, Dubois B, Gallo V, Giacobini E, Gold G, Hurst S,
Lönneborg A, Lovblad K-O, Mattsson N, Molinuevo J-L, Monsch AU, Mosimann
U, Padovani A, Picco A, Porteri C, Ratib O, Saint-Aubert L, Scerri C, Scheltens P,
Schott JM, Sonni I, Teipel S, Vineis P, Visser PJ, Yasui Y, Winblad B (2017):
Strategic roadmap for an early diagnosis of Alzheimer's disease based on
biomarkers. Lancet Neurol 16:661–676.
http://www.ncbi.nlm.nih.gov/pubmed/28721928.
Garcia-Garcia M, Nikolaidis A, Bellec P, Craddock RC, Cheung B, Castellanos FX,
Milham MP (2017): Detecting stable individual differences in the functional
organization of the human basal ganglia. Neuroimage:1–15.
http://linkinghub.elsevier.com/retrieve/pii/S1053811917305979.
Hansson O, Grothe MJ, Strandberg TO, Ohlsson T (2017): Tau Pathology Distribution in
Alzheimer ' s disease Corresponds Differentially to Cognition-Relevant Functional
Brain Networks 11.
Harada R, Ishiki A, Kai H, Sato N, Furukawa K, Furumoto S, Tago T, Tomita N,
Watanuki S, Hiraoka K, Ishikawa Y, Funaki Y, Nakamura T, Yoshikawa T, Iwata R,
Tashiro M, Sasano H, Kitamoto T, Yanai K, Arai H, Kudo Y, Okamura N (2017):
Correlations of (18)F-THK5351 PET with post-mortem burden of tau and
astrogliosis in Alzheimer's disease. J Nucl Med.
http://jnm.snmjournals.org/content/early/2017/08/31/jnumed.117.197426.abstract.
Hoenig MC, Bischof GN, Hammes J, Faber J, Fliessbach K, van Eimeren T, Drzezga A
(2017): Tau pathology and cognitive reserve in Alzheimer's disease. Neurobiol
Aging 57:1–7. http://dx.doi.org/10.1016/j.neurobiolaging.2017.05.004.
Hughes CP, Berg L, Danziger WL, Coben LA, Martin RL (1982): A new clinical scale
for the staging of dementia. Br J Psychiatry 140:566–72.
http://www.ncbi.nlm.nih.gov/pubmed/7104545.
Ikonomovic MD, Abrahamson EE, Ph D, Price JC, Ph D, Mathis CA, Ph D, Klunk WE,
Ph D [ F-18 ] AV-1451 PET retention in choroid plexus : more than " off-target "
binding:2–6.
Jansen WJ, Ossenkoppele R, Knol DL, Tijms BM, Scheltens P, Verhey FRJ, Visser PJ,
Aalten P, Aarsland D, Alcolea D, Alexander M, Almdahl IS, Arnold SE, Baldeiras I,
Barthel H, van Berckel BNM, Bibeau K, Blennow K, Brooks DJ, van Buchem MA,
Camus V, Cavedo E, Chen K, Chetelat G, Cohen AD, Drzezga A, Engelborghs S,
Fagan AM, Fladby T, Fleisher AS, van der Flier WM, Ford L, Förster S, Fortea J,

Foskett N, Frederiksen KS, Freund-Levi Y, Frisoni GB, Froelich L, Gabryelewicz T, Gill KD, Gkatzima O, Gómez-Tortosa E, Gordon MF, Grimmer T, Hampel H, Hausner L, Hellwig S, Herukka S-K, Hildebrandt H, Ishihara L, Ivanoiu A, Jagust WJ, Johannsen P, Kandimalla R, Kapaki E, Klimkowicz-Mrowiec A, Klunk WE, Köhler S, Koglin N, Kornhuber J, Kramberger MG, Van Laere K, Landau SM, Lee DY, de Leon M, Lisetti V, Lleó A, Madsen K, Maier W, Marcusson J, Mattsson N, de Mendonça A, Meulenbroek O, Meyer PT, Mintun MA, Mok V, Molinuevo JL, Møllergård HM, Morris JC, Mroczko B, Van der Mussele S, Na DL, Newberg A, Nordberg A, Nordlund A, Novak GP, Paraskevas GP, Parnetti L, Perera G, Peters O, Popp J, Prabhakar S, Rabinovici GD, Ramakers IHGB, Rami L, Resende de Oliveira C, Rinne JO, Rodrigue KM, Rodríguez-Rodríguez E, Roe CM, Rot U, Rowe CC, Rüther E, Sabri O, Sanchez-Juan P, Santana I, Sarazin M, Schröder J, Schütte C, Seo SW, Soetewey F, Soininen H, Spiru L, Struyfs H, Teunissen CE, Tsolaki M, Vandenberghe R, Verbeek MM, Villemagne VL, Vos SJB, van Waalwijk van Doorn LJC, Waldemar G, Wallin A, Wallin ÅK, Wiltfang J, Wolk DA, Zboch M, Zetterberg H (2015): Prevalence of Cerebral Amyloid Pathology in Persons Without Dementia: A Meta-analysis. Jama 313:1924–1938. http://www.pubmedcentral.nih.gov/articlerender.fcgi?artid=4486209&tool=pmcentrez&rendertype=abstract.

Johnson KA, Schultz A, Betensky RA, Becker JA, Sepulcre J, Rentz D, Mormino E, Chhatwal J, Amariglio R, Papp K, Marshall G, Albers M, Mauro S, Pepin L, Alverio J, Judge K, Philiossaint M, Shoup T, Yokell D, Dickerson B, Gomez-Isla T, Hyman B, Vasdev N, Sperling R (2016): Tau positron emission tomographic imaging in aging and early Alzheimer disease. Ann Neurol 79:110–119.

Jones DT, Graff-Radford J, Lowe VJ, Wiste HJ, Gunter JL, Senjem ML, Botha H, Kantarci K, Boeve BF, Knopman DS, Petersen RC, Jack CR (2017): Tau, Amyloid, and Cascading Network Failure across the Alzheimer's disease Spectrum. Cortex:1–17. http://linkinghub.elsevier.com/retrieve/pii/S0010945217303246.

Landau SM, Harvey D, Madison CM, Koeppe RA, Reiman EM, Foster NL, Weiner MW, Jagust WJ (2011): Associations between cognitive, functional, and FDG-PET measures of decline in AD and MCI. Neurobiol Aging 32:1207–1218.

Landau SM, Lu M, Joshi AD, Pontecorvo M, Mintun MA, Trojanowski JQ, Shaw LM, Jagust WJ (2013): Comparing positron emission tomography imaging and cerebrospinal fluid measurements of ??-amyloid. Ann Neurol 74:826–836.

Lockhart SN, Ayakta N, Winer JR, La Joie R, Rabinovici GD, Jagust WJ (2017): Elevated (18)F-AV-1451 PET tracer uptake detected in incidental imaging findings. Neurology 88:1095–1097. http://www.ncbi.nlm.nih.gov/pubmed/28188303.

Lowe VJ, Curran G, Fang P, Liesinger AM, Josephs KA, Parisi JE, Kantarci K, Boeve BF, Pandey MK, Bruinsma T, Knopman DS, Jones DT, Petrucelli L, Cook CN, Graff-Radford NR, Dickson DW, Petersen RC, Jack CR, Murray ME (2016): An autoradiographic evaluation of AV-1451 Tau PET in dementia. Acta Neuropathol Commun 4:58. http://actaneurocomms.biomedcentral.com/articles/10.1186/s40478-016-0315-6.

Maass A, Landau S, Baker SL, Horng A, Lockhart SN, La R, Rabinovici GD, Jagust WJ, Initiative N (2017): NeuroImage Comparison of multiple tau-PET measures as biomarkers in aging and Alzheimer's disease. Neuroimage 157:448–463.

http://dx.doi.org/10.1016/j.neuroimage.2017.05.058.

Marquié M, Normandin MD, Vanderburg CR, Costantino IM, Bien EA, Rycyna LG,
Klunk WE, Mathis CA, Ikonomovic MD, Debnath ML, Vasdev N, Dickerson BC,
Gomperts SN, Growdon JH, Johnson KA, Frosch MP, Hyman BT, Gómez-Isla T
(2015): Validating novel tau positron emission tomography tracer [F-18]-AV-1451
(T807) on postmortem brain tissue. Ann Neurol 78:787–800.
http://www.ncbi.nlm.nih.gov/pubmed/26344059.

Marquié M, Siao Tick Chong M, Antón-Fernández A, Verwer EE, Sáez-Calveras N,
Meltzer AC, Ramanan P, Amaral AC, Gonzalez J, Normandin MD, Frosch MP,
Gómez-Isla T (2017): [F-18]-AV-1451 binding correlates with postmortem
neurofibrillary tangle Braak staging. Acta Neuropathol:1–10.

Masters CL, Simms G, Weinman NA, Multhaup G, McDonald BL, Beyreuther K (1985):
Amyloid plaque core protein in Alzheimer disease and Down syndrome. Proc Natl
Acad Sci U S A 82:4245–9.
http://www.ncbi.nlm.nih.gov/pubmed/3159021%5Cnhttp://www.pubmedcentral.nih.
gov/articlerender.fcgi?artid=PMC397973.

McKhann G, Knopman DS, Chertkow H, Hymann B, Jack CR, Kawas C, Klunk W,
Koroshetz W, Manly J, Mayeux R, Mohs R, Morris J, Rossor M, Scheltens P,
Carrillo M, Weintrub S, Phelphs C (2011): The diagnosis of dementia due to
Alzheimer's disease: Recommendations from the National Institute on Aging-
Alzheimer's Association workgroups on diagnostic guidelines for Alzheimer's
disease. Alzheimers Dement 7:263–269.

Mishra S, Gordon BA, Su Y, Christensen J, Friedrichsen K, Jackson K, Hornbeck R,
Balota DA, Cairns NJ, Morris JC, Ances BM, Benzinger TLS (2017): AV-1451 PET
imaging of tau pathology in preclinical Alzheimer disease: Defining a summary
measure. Neuroimage 161:171–178.

Mohs RC, Knopman D, Petersen RC, Ferris SH, Ernesto C, Grundman M, Sano M,
Bieliauskas L, Geldmacher D, Clark C, Thal LJ (1997): Development of cognitive
instruments for use in clinical trials of antidementia drugs: additions to the
Alzheimer's Disease Assessment Scale that broaden its scope. The Alzheimer's
Disease Cooperative Study. Alzheimer Dis Assoc Disord 11 Suppl 2:S13-21.
http://www.ncbi.nlm.nih.gov/pubmed/9236948.

Nelson P. T. et al (2013): Correlation of Alzheimer Disease Neuropathologic Changes
With Cognitive Status: A Review of the Literature. J Neuropathol Exp Neurol 2012
May ; 71(5) 362–381 doi101097/NEN0b013e31825018f7 71:362–381.

Ng KP, Pascoal TA, Mathotaarachchi S, Therriault J, Kang MS, Shin M, Guiot M-C,
Guo Q, Harada R, Comley RA, Massarweh G, Soucy J-P, Okamura N, Gauthier S,
Rosa-Neto P (2017): Monoamine oxidase B inhibitor, selegiline, reduces 18 F-
THK5351 uptake in the human brain. Alzheimers Res Ther 9:25.
http://content.wkhealth.com/linkback/openurl?sid=WKPTLP:landingpage&an=0000
1756-199808030-
00031%5Cnhttp://download.springer.com/static/pdf/689/art%253A10.1186%252Fs
13195-017-0253-
y.pdf?originUrl=http%3A%2F%2Falzres.biomedcentral.com%2Farticle%2F10.118
6%2F.

Ossenkoppele R, Schonhaut DR, Schöll M, Lockhart SN, Ayakta N, Baker SL, O'Neil

JP, Janabi M, Lazaris A, Cantwell A, Vogel J, Santos M, Miller ZA, Bettcher BM,
Vossel KA, Kramer JH, Gorno-Tempini ML, Miller BL, Jagust WJ, Rabinovici GD
(2016): Tau PET patterns mirror clinical and neuroanatomical variability in
Alzheimer's disease. Brain 139:1551–1567. http://brain.oxfordjournals.org/.
Ota K, Oishi N, Ito K, Fukuyama H (2015): Effects of imaging modalities, brain atlases
and feature selection on prediction of Alzheimer's disease. J Neurosci Methods
256:168–183.
Palmqvist S, Zetterberg H, Mattsson N, Johansson P, Minthon L, Blennow K, Olsson M,
Hansson O (2015): Detailed comparison of amyloid PET and CSF biomarkers for
identifying early Alzheimer disease. Neurology 85:1240–1249.
Pankov A, Binney RJ, Staffaroni AM, Kornak J, Attygalle S, Schuff N, Weiner MW,
Kramer JH, Dickerson BC, Miller BL, Rosen HJ (2016): Data-driven regions of
interest for longitudinal change in frontotemporal lobar degeneration. NeuroImage
Clin 12:332–340. http://dx.doi.org/10.1016/j.nicl.2015.08.002.
Pedregosa F, Varoquaux G, Gramfort A, Michel V, Thirion B, Grisel O, Blondel M,
Louppe G, Prettenhofer P, Weiss R, Dubourg V, Vanderplas J, Passos A,
Cournapeau D, Brucher M, Perrot M, Duchesnay É (2012): Scikit-learn: Machine
Learning in Python. J Mach Learn Res 12:2825–2830.
http://arxiv.org/abs/1201.0490.
Pfeffer RI, Kurosaki TT, Harrah CH, Chance JM, Filos S (1982): Measurement of
functional activities in older adults in the community. J Gerontol 37:323–9.
http://www.ncbi.nlm.nih.gov/pubmed/7069156.
Rosen WG, Mohs RC, Davis KL (1984): A new rating scale for Alzheimer's disease. Am
J Psychiatry 141:1356–1364,.
Van Rossum IA, Visser PJ, Knol DL, Van Der Flier WM, Teunissen CE, Barkhof F,
Blankenstein MA, Scheltens P (2012): Injury markers but not amyloid markers are
associated with rapid progression from mild cognitive impairment to dementia in
alzheimer's disease. J Alzheimer's Dis 29:319–327.
Scheltens P, Rockwood K (2011): How golden is the gold standard of neuropathology in
dementia? Alzheimer's Dement 7:486–489.
http://dx.doi.org/10.1016/j.jalz.2011.04.011.
Schöll M, Lockhart SN, Schonhaut DR, O'Neil JP, Janabi M, Ossenkoppele R, Baker SL,
Vogel JW, Faria J, Schwimmer HD, Rabinovici GD, Jagust WJ (2016): PET
Imaging of Tau Deposition in the Aging Human Brain. Neuron 89:971–982.
Schwarz AJ, Yu P, Miller BB, Shcherbinin S, Dickson J, Navitsky M, Joshi AD, Devous
MD, Mintun MS (2016): Regional profiles of the candidate tau PET ligand ^{18}F-AV-
1451 recapitulate key features of Braak histopathological stages. Brain:aww023.
http://www.brain.oxfordjournals.org/lookup/doi/10.1093/brain/aww023.
Sepulcre J, Grothe MJ, Sabuncu M, Chhatwal J, Schultz AP, Hanseeuw B, El Fakhri G,
Sperling R, Johnson KA (2017): Hierarchical Organization of Tau and Amyloid
Deposits in the Cerebral Cortex. JAMA Neurol 74:813.
http://archneur.jamanetwork.com/article.aspx?doi=10.1001/jamaneurol.2017.0263.
Smith R, Schain M, Nilsson C, Strandberg O, Olsson T, Hägerström D, Jögi J, Borroni E,
Schöll M, Honer M, Hansson O (2016): Increased Basal Ganglia Binding of 18F-
AV-1451 in Patients With Progressive Supranuclear Palsy. Mov Disord 0:1–7.
Stern Y (2012): Cognitive reserve in ageing and Alzheimer's disease. Lancet Neurol

11:1006–1012. http://dx.doi.org/10.1016/S1474-4422(12)70191-6.

Weiner MW, Veitch DP, Aisen PS, Beckett LA, Cairns NJ, Green RC, Harvey D, Jack

CR, Jagust W, Liu E, Morris JC, Petersen RC, Saykin AJ, Schmidt ME, Shaw L,

Siuciak JA, Soares H, Toga AW, Trojanowski JQ (2012): The Alzheimer's disease

neuroimaging initiative: A review of papers published since its inception.

Alzheimer's Dement 8:S1–S68. http://dx.doi.org/10.1016/j.jalz.2011.09.172.

Xia C, Makaretz SJ, Caso C, McGinnis S, Gomperts SN, Sepulcre J, Gomez-Isla T,

Hyman BT, Schultz A, Vasdev N, Johnson KA, Dickerson BC (2017): Association

of In Vivo [ $^{18}$ F]AV-1451 Tau PET Imaging Results With Cortical Atrophy and

Symptoms in Typical and Atypical Alzheimer Disease. JAMA Neurol 74:427.

http://archneur.jamanetwork.com/article.aspx?doi=10.1001/jamaneurol.2016.5755.

Xia C-F, Arteaga J, Chen G, Gangadharmath U, Gomez LF, Kasi D, Lam C, Liang Q,

Liu C, Mocharla VP, Mu F, Sinha A, Su H, Szardenings AK, Walsh JC, Wang E,

Yu C, Zhang W, Zhao T, Kolb HC (2013): [18F]T807, a novel tau positron emission

tomography imaging agent for Alzheimer's disease. Alzheimer's Dement 9:666–

676. http://linkinghub.elsevier.com/retrieve/pii/S1552526012025320.

 **FIGURES LEGENDS**

 **Figure 1. Mean [$^{18}$F]AV1451 uptake according to diagnosis, amyloid status and**

 **cohort**

 Mean [$^{18}$F]AV1451 SUVR images stratified by amyloid status and disease stage, across

 both the ADNI (top) and BioFINDER (bottom) cohorts.

 **Figure 2. Bootstrap analysis of stable clusters on [$^{18}$F]AV1451 data.** [$^{18}$F]AV1451

 scans were entered into a voxelwise clustering algorithm. The optimal solutions were

 determined using the M-STEPS approach. This resulted in five [$^{18}$F]AV1451 covariance

 networks. These networks were masked with a stability threshold of 0.5, and are

 displayed in the lower half of the figure.

 **Figure 3. Comparison between data-driven and hypothesis-driven ROIs.** Data-driven

 [$^{18}$F]AV1451 covariance networks were compared to previously existing Braak Stage

 ROIs from the literature using descriptive statistics. The clusters were compared to ROIs

 from Schöll, Lockhart et al. and Cho et al using Normalized Mutual Information (top

 left), and were compared to regions from Schwarz et al. using the percentage of Schwarz

 ROI voxels within each data-driven cluster.

 **FIGURE 4. Associations between [$^{18}$F]AV1451 ROIs and global cognition.** General

 linear models comparing [$^{18}$F]AV1451 signal to Global Cognition composite scores were

 run, adjusting for age, sex and education. For each model, a different [$^{18}$F]AV1451 ROI

 was used. ROIs included the five clusters identified in our analysis, as well as Braak

stage regions taken from three different papers: Schöll, Lockhart et al., 2016 *Neuron*; Cho

et al., 2016 *Ann. Neurol.*; Schwarz et al., 2016 *Brain*. Two versions of each Braak ROI

were created, one using regions from that stage only (e.g. Stage 3), and one combining all

regions from that stage with all regions from previous stages (e.g. Stage 1+2+3). The

effect size (t-value) of each tau ROI is shown. AV1451 binding in several ROIs

demonstrated strong relationships with Global Cognition, though only the data-driven

Temporo-parietal region survived multiple comparisons.

**Figure 5. Cumulative ranking of ROI performance across all measures of global**

**cognition and function.** For each measure of global cognition, [$^{18}$F]AV1451 ROIs were

ranked from worst to best (such that the worst region would have rank of 1) with respect

to the effect size of the association between [$^{18}$F]AV1451 in that region and the cognitive

score. The ranks were then summed across all cognitive measurements and are displayed

here. The data-driven Cluster 4 ("Temporo-parietal") ranked the best cumulatively across

cognitive tests, with the data-driven Cluster 3 ("Medial/Inferior/Anterior temporal")

ranking second best.

**FIGURE 6. Lasso regression selects most important features related to cognition.**

All [$^{18}$F]AV1451 ROIs plus age, sex and education were entered into a L1-penalized

Lasso regression feature selection routine with the Global Cognitive composite score as

the dependent variable. The Lasso selected education and two ROIs: the data-driven

Temporo-parietal region, and the Schwarz Single VI region. Together in a general linear

model, these features explained 28% of the variance in the Global Cognition score.

 **TABLES**

 **Table 1: Demographic information, MMSE scores and amyloid-positivity rates**

|  | Controls | | MCI | | AD | | Total | |
|---|---|---|---|---|---|---|---|---|
|  | **BioF** | **ADNI** | **BioF** | **ADNI** | **BioF** | **ADNI** | **BioF** | **ADNI** |
| **n** | 55 | 43 | 21 | 37 | 47 | 10 | 123 | 90 |
| **Age (SD)** | **75.0 (6.2)** | **70.3 (5.9)** | 70.8 (10.9) | 72.0 (6.8) | 70.1 (8.6) | 73.3 (4.3) | 72.4 (8.4) | 71.3 (6.1) |
| **% Male** | 50.9% | 46.5% | 57.1% | 67.6% | 55.3% | 60.0% | 53.7% | 56.7% |
| **Education (SD)** | **12.0 (3.7)** | **16.1 (2.4)** | **11.7 (3.7)** | **16.9 (2.7)** | **12.2 (3.2)** | **15.0 (3.0)** | **12.0 (3.5)** | **16.3 (2.6)** |
| **% Amyloid+** | 43.6% | 33.3% | **100%** | **44%** | 100% | 100% | **73.3%** | **44.8%** |
| **MMSE (SD)** | 29.1 (1.1) | 29.0 (1.3) | **25.7 (2.8)** | **28.4 (2.0)** | **21.2 (5.1)** | **25.5 (5.1)** | **25.5 (4.9)** | **28.3 (2.5)** |

840    •   * **BOLD** text indicates significant difference (p<0.05) between cohorts, as
841         measured by t-test, or Fisher's Exact Tests
842    •   ADNI = Alzheimer's Disease Neuroimaging Initiative; BioF = BioFINDER,
843         MMSE = Mini-Mental State Examination; SD = Standard Deviation

**FIGURES**

Figure 1

Figure 2

872    Figure 3

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875    Figure 4
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881    Figure 5

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883    Figure 6

885 **SUPPLEMENTARY**
886
887 **Table S1. Best-ranking AV1451 ROIs at describing global cognition across different**
888 **cognitive tests**

| | MMSE | | | CDRSB | | |
|---|---|---|---|---|---|---|
| **Rank** | **Study** | **ROI** | **t** | **Study** | **ROI** | **t** |
| 1 | Data-driven | Temporo-parietal | -2.45* | Schwarz | Stage I | 3.60** |
| 2 | Data-driven | Temporal | -2.00* | Data-driven | Temporo-parietal | 3.49** |
| 3 | Cho | Single IV | -1.97 | Cho/Scholl | Stage I | 3.49** |
| 4 | Cho | Stage IV | -1.83 | Data-driven | Temporal | 3.33** |
| 5 | Other | Inferior Temporal | -1.80 | Cho | Stage IV | 3.18* |

| | ADAS11 | | | ADAS13 | | |
|---|---|---|---|---|---|---|
| **Rank** | **Study** | **ROI** | **t** | **Study** | **ROI** | **t** |
| 1 | Data-driven | Temporo-parietal | 4.10** | Data-driven | Temporo-parietal | 3.02* |
| 2 | Schwarz | Stage I | 3.50** | Schwarz | Stage I | 2.57* |
| 3 | Cho | Single IV | 3.43** | Data-Driven | Temporal | 2.35* |
| 4 | Data-driven | Temporal | 3.39** | Cho/Scholl | Stage I | 2.34* |
| 5 | Cho | Stage IV | 3.33** | Cho | Single IV | 2.34* |

| | ECOG | | | FAQ | | |
|---|---|---|---|---|---|---|
| **Rank** | **Study** | **ROI** | **t** | **Study** | **ROI** | **t** |
| 1 | Data-driven | Temporo-parietal | 3.68** | Schwarz | Stage I | 2.91* |
| 2 | Cho | Stage IV | 3.48** | Data-driven | Temporal | 2.69* |
| 3 | Schwarz | Stage I | 3.40** | Cho/Scholl | Stage I | 2.68* |
| 4 | Cho | Single IV | 3.40** | Data-driven | Temporo-parietal | 2.67* |
| 5 | Data-Driven | Temporal | 3.40** | Cho | Stage III | 2.63* |

889 * $p<0.05$ ** p[Bonf.]<0.05
890 ROI = Region of Interest; MMSE = Mini-Mental State Examination; CDRSB = Clinical
891 Dementia Rating Sum of Boxes; ADAS = Alzheimer's disease Assessment Scale; ECog
892 = Everyday Cognition; FAQ = Functional Activities Questionnaire

899 **Table S2. Fitted values from the General Linear Model comparing selected AV1451 ROIs to**
900 **Global Cognition composite also explains variance in individual cognitive tests.**

| Test | $R^2$ |
|------|-------|
| CDRSB | 0.214 |
| ADAS11 | 0.261 |
| ADAS13 | 0.215 |
| FAQ | 0.221 |
| ECog | 0.196 |
| MMSE | 0.219 |

901 MMSE = Mini-Mental State Examination; CDRSB = Clinical Dementia Rating Sum of
902 Boxes; ADAS = Alzheimer's disease Assessment Scale; ECog = Everyday Cognition;
903 FAQ = Functional Activities Questionnaire
904
905

906 **Table S3. Variables selected by Lasso regression that optimally described global**
907 **cognition across different cognitive tests**

| MMSE | | CDRSB | | ADA |
|------|-----|-------|-----|-----|
| Study | ROI | Study | ROI | Study |
| Data-driven | Temporo-parietal | Data-driven | Temporo-parietal | Data-driven |
| Data-driven | Subcortical | | | Schwarz |
| Schwarz | Stage VI | | | Schwarz |
| Demographic | Education | | | Demographic |

| ADAS13 | | ECOG | | F |
|--------|-----|------|-----|---|
| Study | ROI | Study | ROI | Study |
| Data-driven | Temporo-parietal | Data-driven | Temporo-parietal | Data-driven |
| Schwarz | Single VI | | | Schwarz |
| Schwarz | Stage I | | | Schwarz |
| Schöll | Single II | | | Demographic |
| Demographic | Education | | | |
| Demographic | Age | | | |

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910 MMSE = Mini-Mental State Examination; CDRSB = Clinical Dementia Rating Sum of
911 Boxes; ADAS = Alzheimer's disease Assessment Scale; ECog = Everyday Cognition;
912 FAQ = Functional Activities Questionnaire

920 **Table S4. Disparities in Braak stage regions-of-interests across studies**

| Brain Region | Schöll, Lockhart et al. | Cho et al. | Schwarz et al. | Data-driven |
|---|---|---|---|---|
| **Hippocampus** | Included | Not included | Head only | Head only |
| **Lingual Gyrus** | Stage 3 | Stage 5 | Stage 6 | TP/US |
| **Thalamus** | Stage 4 | Not included | Not Included | SCN |
| **Putamen** | Stage 5 | Not included | Not Included | MAIT |
| **Lateral Occipital** | Stage 5 | Stage 5 | Stage 4 | TP/US |
| **PCC** | Stage 4 | Stage 5 | Not Included | TP |
| **Insula** | Stage 4 | Stage 5 | Not Included | MAIT |
| **Frontal Lobe** | All stage 5 | All stage 5 | Not Included | F/TP |

922 TP = Temporo-parietal; US = Unimodal Sensory; SCN = Subcortical/Noise; MAIT =
923 Medial/Anterior/Inferior Temporal; F = Frontal
924