Hemispheric asymmetry of globus pallidus relates to alpha modulation in reward-

related attentional tasks

Subcortical modulation of visual alpha oscillations

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Abstract

While subcortical structures such as the basal ganglia (BG) have been widely explored in relation to motor control, recent evidence suggests that their mechanisms extend to the domain of attentional switching. We here investigated the subcortical involvement in reward related top-down control of visual alpha-band oscillations (8 – 13 Hz), which have been consistently linked to the mechanisms supporting the allocation of visual spatial attention. Given that items associated with contextual saliency (e.g. monetary reward or loss) attract attention, it is not surprising that alpha oscillations are further modulated by the saliency properties of the visual items. The executive network controlling such reward-dependent modulations of oscillatory brain activity has yet to be fully elucidated. Although such network has been explored in terms of cortico-cortical interaction, it likely relies also on the contribution of subcortical regions. To uncover this, we investigated whether derived measures of subcortical structural asymmetries could predict interhemispheric modulation of alpha power during a spatial attention task. We show that volumetric hemispheric lateralization of globus pallidus (GP) and thalamus (Th) explains individual hemispheric biases in the ability to modulate posterior alpha power. Importantly, for the GP, this effect became stronger when the value-saliency parings in the task increased. Our findings suggest that the Th and GP in humans are part of a subcortical executive control network, differently involved in modulating posterior alpha activity. Further investigation aimed at uncovering the interaction between subcortical and neocortical attentional networks would provide useful insight in future studies.

Introduction

Within the domain of spatial attentional allocation, the involvement of neocortical networks has been extensively studied. However, there is also growing evidence pointing to the role of subcortical areas extending into higher level cognitive functions.

In order to efficiently operate in natural environments, our brains must rely on neuronal mechanisms which selectively gate stimuli by prioritizing relevant information while reducing the interference of distractors [1]. It is well established that deployment of attentional resources is biased towards stimuli associated with salience (e.g. monetary reward or loss), even when unrelated to the current task goals [2]. Converging evidence has shown that modulations of posterior neuronal oscillations in the alpha band (8 – 13 Hz) reflect the allocation of covert attention [3–5]. In particular, a selective suppression of alpha-band oscillations is observed over visual areas contralateral to the attended hemifield, while a relative increase occurs ipsilaterally [5]. It is now clear that the dorsal attention network (DAN) plays a crucial role in the modulation of alpha band activity in spatial attention tasks [6–10]; however, the involvement of subcortical regions in such modulation is yet to be fully uncovered. Previous literature has indeed linked subcortical activity to cognitive control[11–13], but remains to be elucidated whether subcortical areas – in coordination with the DAN – exert top-down control over posterior alpha band oscillations.

Activity from such subcortical regions are not likely to be detectable with magnetoencephalography (MEG) due to the lower sensitivity of the technique to deeper structures in the brain. As an alternative, recent studies have succeeded in relating structural brain properties derived from magnetic resonance imaging (MRI) to the ability to modulate oscillatory brain activity, measured by MEG [14,15]. For instance, it has been demonstrated that individual hemispheric asymmetries in the volume of the superior longitudinal fasciculus (SLF) [8], a white matter tract connecting fronto-parietal regions, was related to the

individual ability to modulate alpha oscillations in visual cortical regions. Importantly, the

study demonstrated that subjects with greater right than left SLF volume were also the ones

displaying higher modulation of posterior alpha activity in the left hemisphere, compared to

the right (and vice versa). Through an analogous approach, we postulated that volumetric

asymmetries of subcortical areas would be reflected by individual interhemispheric biases in

the modulation of alpha oscillations during selective attention in a reward context. Basal

ganglia (BG), in addition to motor control, have a well-established role in reward processing

and salience attribution [13,16–18], although recent evidence has already pointed to their

functions extending into higher level cognitive processing. This notion has been initially

explored in animal recordings [19–24], while in humans, it has recently been suggested that

the BG play also a specific role in spatial attention and selection [25–27]. Consistent with

these lines of evidence, volumetric abnormalities related to the BG have been associated with

symptoms of inattention in attention deficit and hyperactivity disorder (ADHD) [28–30] and

with aberrant salience attribution abilities in patient with schizophrenia [31–35].

On the other hand, other subcortical structures such as the thalamus, have been involved in

the regulation of synchronized activity in the visual cortex in relation to visual attentional

processes [36,37]. Similarly to the premises in [8], we here assumed that a larger subcortical

volume would reflect higher control over alpha oscillations in a hemispheric-specific fashion.

To investigate this hypothesis we made use of data from a recent study that considered the

impact of stimuli paired with value salience on the modulation of oscillatory brain activity in

a covert attention task [38]. MEG data were recorded while participants performed a spatial

cueing task in which Chinese symbols served as targets and distractors. Prior to the

recordings, stimuli were paired with monetary rewards or losses. Alpha power modulation

was shown to be influenced by the salience of the targets and distractors, but not their valence

(i.e., reward and loss had the same effect). We here re-analysed these data with the aim to

investigate the putative role of the subcortical brain areas in biasing alpha power modulation

during attentional shifts to stimuli paired with value-saliency. MRI data of the same

participants were processed in order to estimate volumetric asymmetries of subcortical areas,

consistent with methods employed in previous studies on clinical and healthy population

[32,34,39]. We focused on identifying the link between individual volumetric asymmetries of

the subcortical areas and individual interhemispheric bias in the ability to modulate posterior

alpha oscillations. Crucially, we further examined whether this relationship was affected by

the degree of stimulus-value associations in the task [40].

Results

We acquired structural and electrophysiological data from 25 participants. Participants'

performance was tested during a covert attention paradigm, where Chinese symbols served as

targets and distractors (Figure 1). During a learning phase, prior to the actual task, the stimuli

were associated with different values (positive, negative or neutral). In the testing phase, a

central cue probed an upcoming contrast variation of the target, which appeared either at

1450 or 2350 ms, predicting its position in 95% of the trials. Participants were instructed to

indicate, with button press, the direction of the contrast change, which could either increase

or decrease with equal probability. MEG data, eye-tracking and behavioural responses were

acquired during the testing phase. Time-frequency representations of power were calculated

from MEG trials after preprocessing and artifacts rejection. Power modulation (MI) indices

were computed by contrasting power in trials where participants were validly cued to the

right (*attend right* trials) with trials where participants were validly cued to the left (*attend*

left trials) (see Eq.(1), *Materials and Methods*). As presented in the previously reported

results [38], we confirmed that participants displayed a clear modulation of alpha band

activity in parieto-occipital sensors ($MI(\alpha)$): when covertly orienting attention to the cued

side, alpha power decreased in the contralateral hemisphere while it increased relatively in

the ipsilateral hemisphere (Figure 2A). The magnitude of alpha power modulation, as

reflected by $MI(\alpha)$, progressively increased until the target changed contrast (Figure 2B). To

best quantify the modulation, we focused our analysis on the 750 ms interval immediately

preceding the onset of the contrast change. Next, right and left ROIs were identified as

clusters of symmetric pairs of sensors showing the highest alpha lateralization values (see

Materials and Methods) (i.e., sensors displaying highest interhemispheric difference in alpha

modulation).

Starting from the assumption that, to a certain extent, an inter-subject variability in the ability

to modulate alpha power – in absolute value – must exist in the right compared to the left

hemisphere (and vice versa), we sought to quantify individual hemispheric biases in the

ability to modulate alpha activity. To this purpose, hemispheric lateralized modulation of

alpha power (HLM(α)) values were then computed for each participant by summing the

average MI(α) in the right and left hemisphere ROIs (see Eq.(2), *Materials and Methods*). As

a result of this computation, positive HLM(α) values would demonstrate that a given subject

was better at modulating their right, compared to left, hemisphere alpha power, while a

negative index would reflect higher ability to modulate alpha power on their left, compared to

right, hemisphere. The histogram in Figure 2B depicts the distribution of hemispheric biases

related to attentional modulation of alpha power. HLM(α) indices ranged from about -0.1 to

0.1 (i.e. a 20% variation) but they were normally distributed around zero across participants

(Shapiro Wilk, $W = .958$, $p = .392$).

Volumetric asymmetry of basal ganglia in relation to hemispheric lateralized alpha

modulation

The next step was to determine whether the biases in the ability to modulate left versus right

hemisphere alpha (HLM(α)) was related to individual hemispheric lateralization of

subcortical structures. A semi-automated segmentation tool implemented in FMRIB's

Software Library (FSL), was used to estimate volumes for the left and right subcortical and

limbic structures, namely: Globus Pallidus (GP), Nucleus Accumbens (Acb), Caudate

Nucleus (CN), Putamen (Pu), Hippocampus (Hpc), Amygdala (Am) and Thalamus (Th). We

then calculated the hemispheric lateralized volumes (LV) for each set of structures (see

Materials and Methods, Eq.(3)). Positive (or negative) LV$_s$ values, for a given participant,

indicated whether a specific substructure s was larger in the right compared to the left

hemisphere (and vice versa). Further analysis revealed that, over subjects, the Acb and Th

were significantly left lateralized ($z = -3.78$, $p = 1.56\times10^{-4}$ and $z = -3.59$, $p = 3.28\times10^{-4}$,

respectively; two-sided Wilcoxon signed rank test), whilst the CN was right lateralized ($z =$

2.97, $p = .003$). For the other substructures, no significant lateralizations were identified.

These significant lateralization biases in the Acb, Th and CN are of potential interest but will

not be further considered in the context of this study. Given the volumetric variability in the

set of substructures considered for the segmentation protocol, we performed a cross

correlation analysis between the different substructures, including left and right volumes, to

query about whether there might be a bias in the segmentation protocol. No significant effects

were found (positive or negative correlations, all *p-values* >0.688; highest negative

correlation $R=-.084$) indicating that, if a given structure is larger for a given subject, this

doesn't imply a bias in the segmentation protocol (e.g. to the expense of neighbouring,

allegedly smaller areas).

To investigate whether individual subcortical asymmetries (LVs, as defined in Eq. (3))

predicted differences in hemispheric lateralized modulation of alpha power (HLM(α)), we

implemented a GLM, where LV indices were included as multiple explanatory variables for

the response variable (individual HLM(α)). A significant regression was found: when

considering the grand average of all conditions, a linear combination of the subcortical LVs

was able to explain HLM(α) values ($F_{7,17} = 3.37$, $p = .019$, adjusted $R^2 = .409$). When

assessing each predictor individually, only the beta coefficients for LV_{GP} and LV_{Th} were

found to be significantly higher than zero (partial correlation: $p = .004$ and $p = .028$) (Figure

4A). Hence, when controlling for the other explanatory variables in the model, only GP and

TH asymmetry ($LV_{GP,}$ LV_{TH}) significantly contributed to explain biases in hemispheric

lateralized alpha band modulation ($\beta = 1.768$ and $\beta = 1.924$, respectively). The independent

contribution of GP and TH lateralization is visible in Figure 4B,C showing the partial

regression plots for LV_{GP} and LV_{TH} in relation to the HLM(α) values. We conclude that

hemispheric biases in GP and TH volume are predictive of the individual abilities to

modulate left versus right hemisphere alpha. Precisely, subjects presenting a larger GP

volume in the left hemisphere compared to the right, also displayed a higher ability to

modulate alpha power (in absolute value) in the left visual hemisphere compared to the right

(and vice versa); the same association holding for the Th in relation to HLM(α) values.

Hemispheric asymmetry of globus pallidus correlates selectively with power modulation in

the alpha band

In order to better interpret the GLM results, we assessed whether the linear relationship

arising from the model was restricted to the alpha band: to this end, a non-parametric

approach was implemented to further explore the LV_{GP} and LV_{TH} in relation to HLM(α).

This method allows circumvention of the multiple comparison problem over frequency and

time points by evaluating the full low-frequency spectrum (2-30 Hz) from -750 to 0ms [41].

We therefore conducted a cluster-based permutation test using a dependent samples

regression t-statistic to evaluate the effect (linear association between $LV_{GP/TH}$ indices and

HLM over all frequencies) at the sample level. A p-value of .05 was chosen for thresholding

the t-statistic of the permutation distribution and a critical value corresponding to alpha =

.025 (two tailed) was considered for the cluster-level regression test statistic. As depicted in

Figure 5A, we observed a significant cluster (p = .004) extending for the entire 750 ms

window of interest (i.e., when covert attention was deployed to the cued stimulus before the

contrast changed), which confirmed a positive linear association (positive t-value) between

LV_{GP} asymmetry and hemispheric lateralized modulation (HLM) of power constrained to the

alpha frequency range. When applying the same analysis to the Th asymmetry in relation to

HLM, no significant clusters of sensors were identified.

Hemisphere specific relations between alpha modulation and GP asymmetry.

Given the specific association found between LV_{GP} and HLM(α), arising from the previous

analysis, we decided to further investigate the hemisphere-specific influence of GP

volumetric asymmetry on alpha modulation indices. For this purpose, we sought to compare

average left and right hemisphere MI(α)s of participants according to the direction of GP

lateralization. This was done by means of median split of the LV_{GP} distribution, hence

resulting in two subgroups, that either had a bias towards a larger left than right GP volume

or vice versa (see *Materials and Methods*). A topographical representation of MI(α) values

together with a bar plot of MI(α) averaged across right and left hemisphere ROIs per each

subgroup is shown in Figure 1S. Consistent with the GLM results, participants with a larger

right than left GP, also displayed a higher modulation of alpha band (in absolute value) in the

right hemisphere compared to the left. Given that the assumption of normality, necessary to

perform a mixed-effect ANOVA, was not met for the distribution of MI(α) indices in the two

subgroups, we implemented a non-parametric cluster-based permutation test to compare the

MI(α) between the two aforementioned subgroups (averaged across specific time and

frequency band of interest), employing an independent sample t-test score, and then

comparing it with the resulting permutation distribution. This allowed us to explore whether

there was a hemispheric-specific difference in the two subgroups in the extent of absolute

alpha modulation. The test indicated a significant cluster of sensors over right posterior

channels (p= .027), hence including the previously defined right ROI and denoting a

significant difference in the right hemisphere absolute alpha modulation (MI(α)) between the

two subgroups. These results might suggest that the linear association arising from the GLM

(Figure 4A, B) in relation to the association between LV_{GP} and HLM(α), was largely driven

by right hemisphere alpha modulation. We conducted the analogous analysis performing a

median split of the distribution of LV_{TH} indices. In that case we did not find interhemispheric

dominance in alpha modulation indices related to lateralization of the thalamus in the right

compared to left hemisphere.

The involvement of globus pallidus and thalamus in relation to stimulus-value associations

Crucially, we aimed at assessing whether the level of value-saliency occurrences (VO) in a

given trial influenced the association between the structural and functional lateralization

indices arisen from the GLM. We first calculated HLM(α) (see Eq.(2), *Materials and*

Methods) values for each participant, separately for the three VO levels, namely two, one and

zero value saliency occurrences (see *Materials and Methods*). We then examined Pearson

correlations between HLM(α) and LV values for both GP and Th, which showed a positive

significant β in the model, across the three levels considered (Figure 6). LV_{GP} significantly

correlated with HLM(α) only in trials where both target and distractors had value-salience

(two VO) ($r = .68$, $p=1.75 \times 10^{-4}$; Figure 6A). This denotes that, in trials with two value-salient

items presented, participants exhibiting a right lateralized GP volume, also displayed a

stronger alpha modulation in the right compared to the left hemisphere, and vice versa. LV_{GP}

did not significantly correlate with HLM(α) when only one or none of the stimuli presented

were associated with a salient value ($p = .144$ and $p = .314$, respectively; Figure 6A).

In order to statistically quantify the influence of the stimulus-value association on the

relationship between LV_{GP} and HLM(α), we compared *robust correlations* in the three

conditions according to the bootstrap method described in [42] for dependent overlapping

correlations (see *Materials and Methods*). The correlation between LV_{GP} and HLM(α) in

trials with two occurrences of value-salience, significantly differed both from the condition

characterized by one (95% CI [.106, .672]) and zero occurrences (95% CI [.125, .897]). This

confirmed that the association between lateralized GP volume and alpha modulation bias

significantly increased as a function of the number of value-salient occurrences in the task

(Figure 6B). We performed the same analysis in order to assess whether value-saliency

occurrences mediated also the association between LV_{TH} and HLM(α). When considering the

correlation indices in the three conditions separately, no significant linear relationship was

found between the two indices (Figure 7A). Also in this case, when comparing robust

correlations between the three conditions, according to the same method above, no significant

difference was found. This suggested that the relationship between thalamus volumetric

lateralization and alpha modulation arising from the model in Eq.(3), was not driven by the

number of value-salient occurrences in the task.

Behavioural analysis

We also investigated whether subjects displayed a spatial bias in task performance,

irrespective of the value-saliency levels. To this end we performed a paired t-test to assess

whether participants' performance differed between left and right cued trials, in both reaction

times (RT) and accuracy measures. No behavioural spatial bias was found neither in RT

(p=.341) nor in accuracy (p=.572) values. Secondly, we examined whether value-salient

occurrences (VO) levels, modulated participants' behavioural performance.

We then compared mean RT and accuracy for the three VOs levels (see *Materials and*

Methods). There were no statistically significant differences between the three groups, as

determined by one-way ANOVA, in RT ($F_{(2,72)}$ =.004, *p*=.995) (Figure 8A) nor in accuracy

($F_{(2,72)}$=.003, *p*=.996) (Figure 8C). We then tested whether a behavioural spatial bias occurred

across value saliency occurrences (i.e., whether subjects displayed a difference in RT or

accuracy asymmetry across VOs). We computed measures of behavioural asymmetry in

accuracy (BA_{ACC}) and reaction times (BA_{RT}) (see Eq.(5), *Materials and Methods*).

Analogously to the method used to compute HLM(α), we created asymmetry indices for

every subject by contrasting behavioural measures for *attend right* with *attend left* trials. As

such, a positive BA_{RT} would indicate that subjects were faster when cued to the left compared

to the right hemisphere, and vice versa. Similarly, positive BA_{ACC} indices reflected higher

accuracy when cued to the right compared to the left hemisphere. With the method

aforementioned, we performed a one-way ANOVA to assess whether a significant difference

in behavioural bias occurred across the three VO conditions. Neither BA_{RT} nor BA_{ACC} values

significantly differed across VOs ($F_{(2,72)}$=.191, *p*=.826 and $F_{(2,72)}$=.669, *p*=.515, respectively)

(Figure 8B, 8D). With the aim of determining a potential link between lateralized indices of

behavioural performance and the anatomical (LVs) and functional (HLM(α)) lateralization

indices of interest, we employed three separate GLMs to assess whether a linear combination

of BA_{RT} and BA_{ACC} values could explain LV_{GP}, LV_{TH} and/or HLM(α) indices. Neither LV_{GP}

nor LV_{TH} could be explained by the behavioral lateralized measures ($F_{1,23}$=.18, *p*=.834,

adjusted R^2=-.07 and $F_{1,23}$=.16, *p*=.849, adjusted R^2=-.07). The same result held for the

prediction of HLM(α), yielding also in this case no significant regression coefficients

($F_{1,23}$=1.17, p=.33, adjusted R^2=-.01).

Last, we investigated whether individual behavioral spatial biases could be accounted for by

a combination of the other measures examined. To this end, we considered all subcortical

LV$_S$ and HLM(α) indices and specified them as regressors in a general linear model (see

Eq.(6), *Materials and Methods*), in order to determine whether they could explain biases in

RT and accuracy (BA$_{RT}$ and BA$_{ACC}$). No significant regression was found which could

account for BA$_{RT}$ indices ($F_{8,16}$=.85, p=.570, adjusted R^2=-.05) nor for BA$_{ACC}$ indices

($F_{8,16}$=1.07, p=.429, adjusted R^2=-.023, respectively). (Figure 2S). The lack of a relationship

between spatial bias in task performance and functional and structural hemispheric

lateralization indices is likely explained by the orthogonalization of attentional orienting and

stimulus-value associations, in line with the null findings in [38].

Discussion

The aim of this study was to investigate the involvement of subcortical structures in modulating spatial attention to stimuli associated with contextual salience. In particular, we investigated volumetric measures of subcortical structures in relation to the ability to modulate visual alpha oscillations in the framework of an attentional task with a reward component [43,44]. We made use of a previous dataset in which alpha activity was modulated by both spatial attention and value-salience associations[38]. We first observed that volumetric lateralization of subcortical areas explained individual differences in the ability to modulate interhemispheric alpha power. More specifically, participants exhibiting a right lateralized GP also had a better ability to modulate posterior alpha oscillations in the right compared to left hemisphere, and vice versa. The same association held for the relationship between Th and alpha modulation. For the GP, we were able to show how this association was significantly constrained to the alpha frequency band. Importantly, we showed that the association between GP and alpha hemispheric lateralized modulation increased as a function of value-saliency occurrences in the task: the correlation between GP lateralized volume and alpha modulation asymmetry was significantly higher in trials where both target and distractor were represented by a salient item (reward or loss) as compared to one or zero salient items. With respect to the Th and its association to interhemispheric alpha power modulation, no relation to saliency was found. To the best of our knowledge, this is the first finding relating individual volumetric differences in BG and thalamus to the modulation of posterior alpha oscillations.

Subcortical areas and alpha synchronization

Our first finding is in line with a growing body of literature demonstrating a subcortical involvement in high level cognitive functions, such as conscious perception [45], working

memory performance [46], cognitive control [47–49] and attentional control [50,51]. Specific

to attentional control, we showed that volumetric asymmetry of the subcortical areas

considered predicts individual biases in the ability to efficiently allocate attention towards a

cued target, as indexed by interhemispheric modulation of alpha power. This is strong

evidence in favor of a subcortical involvement in attentional processing, given the well-

established role of neuronal synchronization in the alpha band into the selective gating of

relevant information during visuospatial covert attention tasks [52,53]. Although the

functional association between BG and cognitive control in the context of reward has been

already investigated [54,55], we here provide novel insights into the involvement of

subcortical regions in the modulation of posterior alpha oscillations.

Pulsed inhibition

A well-recognized function of the BG is to inhibit or promote cortical activity via

GABAergic signalling, through the globus pallidus pars interna (GPi), one of its major output

structures [56,57] (see below for a discussion of potential pathways). The BG might then

exercise its influence by applying control over activity in the prefrontal cortex or it might

directly coordinate posterior regions (as reflected by its relationship to alpha power

modulation during reward processing). Our results suggest that individual differences in GP

volume lateralization may correspond to interhemispheric variability in GABAergic

signalling and thus reflect the subcortical potential to inhibit cortex. This input is likely

responsible for producing the mechanisms of 'pulsed inhibition' in the visual cortex [52],

reflected by interhemispheric modulation of alpha power, allowing the selective processing

of stimuli. Implicitly, we assumed that the volume of the GP indirectly reflects its ability to

exert its top-down control over posterior areas, its size possibly representing a determinant

for the number of GABAergic neurons involved in the control mechanism.

GP in relation to attentional selection and cognitive control

Interestingly, our results emphasize the specific contribution of the GP in supporting

stimulus-driven allocation of attention in a value-based context. The GPi is considered to

mediate the output of the BG. Previous literature has implicated this structure in voluntary

movement regulation: its functions have indeed been predominantly investigated in clinical

and animal models in association with motor functions and action control [12,58], describing,

for instance, reduction of hypokinetic and rigidity symptoms following pallidotomy in

humans [59,60] and abnormal pallidal activity in monkeys with induced parkinsonism[58].

Nevertheless, recent results from single unit recordings in humans have provided indications

that electrophysiological activity in the GPi reflects processing of stimuli associated with

different reward contingencies [61]. This is corroborated by evidence of alterations of

cognitive, in addition to motor, abilities, following pallidotomy in Parkinson's disease

patients [62]; In addition, GPi DBS in the treatment of Parkinson's desease has been reported

to be associated with several cognitive impairments, such as subtle declines in attention and

concentration, although to a lesser extent when compared to subthalamic (STN) DBS [63].

This aspect has been further addressed in clinical studies showing a link between Parkinson's

disease, associated with abnormal pallidal activity [60,64], and altered reward processing as

well as updating [65,66]. Structural GP abnormalities have also been linked to impaired

suppression of distractors in ADHD [28,67] as well as psychotic symptoms in schizophrenia

[31,33,68], which has been related to aberrant salience attribution and reward learning

[34,69]. As an important output component of the reward circuit [70], the GPi might serve to

indirectly influence the cortical information flow by biasing selective processing of value-

related stimuli. Our data suggest that this influence is further reflected by a modulation of

alpha band activity.

Right lateralization of the association between GP and alpha modulation

Interestingly, as visible in Figure 1S, the association between GP lateralization and interhemispheric alpha power was largely related to right hemisphere differences in absolute alpha modulation between subjects exhibiting a right, as compared to left, lateralized GP volume. This finding possibly reflects and is explained by the right hemisphere dominance allegedly characterizing spatial attention processes [71], corroborated by the right lateralized feature of the ventral attentional network, which has been described as specifically involved in the processing of behaviourally salient stimuli [43]

Differential role of GP and Th in relation to posterior alpha modulation

Our results show that GP and Th lateralizations were related to the interhemispheric bias in alpha modulation during selective allocation of attention. However, only GP lateralization, and not Th lateralization, was related to the value-saliency pairings in the task. The different contribution from GP and Th in relation to saliency occurrences is likely to reflect different roles of the two networks in the top-down control of attentional processing. The GP provides a modulatory signal related to the processing of stimuli that draw attention due to their strong saliency associations. The perceptual competition resulting from attending to a salient target whilst required to suppress an equally salient distractor, might be resolved by a network involving the GP. Increased midbrain activity has indeed been shown to accompany attentional suppression of a highly rewarding distractor carrying a strong perceptual competition with the target [72], suggesting that dopaminergic networks might flexibly modulate attentional selection in reward-related contexts.

The correlation between Th lateralization and attention-related alpha modulation, which was irrespective of the saliency component in the current task, is in line with the notion that thalamic activity, particularly arising from its largest nucleus, the pulvinar, modulates the

alpha rhythm in extended visual areas [36,37,73–75]. The pulvinar was first shown to

contribute to the generation of the posterior alpha rhythm in dogs [36] and also to regulate

synchronized activity between visual cortical areas to support the allocation of attention in

human and nonhuman primates [74–77]. Our findings, therefore, add to the growing body of

evidence suggesting that thalamo-cortical interactions play a fundamental role in shaping

cognitive processing [23,75,78,79]

Pallido-cortical pathways

Through which route does the GP influence visual alpha oscillations? A possibility is that the

GP modulates prefrontal activity which in turn engages and affects dorsal attentional

networks [11,80]. The dorsal attention network, with the intraparietal sulcus (IPS) and frontal

eye-fields (FEF) as its major hubs, has been suggested to mediate top-down allocation of

attention. Supporting this notion, both the IPS and FEF have been causally implicated in the

control over posterior alpha oscillations in relation to attentional shifts [6–8,43,81]. With our

results, we propose the existence of a brain network which allows salience driven signals

from the BG to influence the prefrontal cortex in biasing the competition among posterior

regions. The idea of a BG-cortico loop involved in stimulus driven reorienting of attention

has been already introduced [16,82] and is consistent with the notion of a 'salience network',

which integrates behaviourally relevant input in order to bias and guide cognitive control

[83–86]. Within this framework, the BG, through their main output via the GPi, are thought

to influence the connectivity between frontoparietal regions by updating goal-directed

behaviour, in order to adapt to changes in the environment [87].

The influence of GP on posterior alpha oscillations could be mediated through indirect

projections via the thalamus. The major target of GPi projections is the motor thalamus,

including ventrolateral and ventral anterior thalamic nuclei, which innervates motor and

premotor cortex [56,88,89]. However, cortical projections from thalamic nuclei receiving

input from the BG might be more diverse and also target prefrontal areas [90], which would

enable an indirect modulation of frontoparietal networks by the GPi via the thalamus.

Additionally, intra-thalamic connectivity [91,92] as well as complex interactions between the

thalamic reticular nucleus and thalamic nuclei [93,94] may provide multiple alternative

pathways to convey influence of the GPi on cortical areas and modulate behavior [95]. Note

that these pallido-thalamo-cortical pathways are not necessarily related to the volumetric

hemispheric lateralization of the thalamus reported here, but might instead represent

independent pathways.

Another 'pallido-frontal' pathway has recently been suggested by Saunders et al. [96],

describing specific connections between the external Globus Pallidus (GPe) and prefrontal

areas. The authors suggests to extend traditional BG-prefrontal cortex models, by the

introduction of a subdivision of GPe cells based on their differential cholinergic marker

expression. Employing in vivo extracellular recordings in mice coupled with optogenetics,

they demonstrate a direct modulation of frontal cortex by non-cholinergic GPe neurons. Such

a projection bypasses canonical BG-cortical networks involving thalamic nuclei. It is

interesting to note that the paradigm employed in [96] focused on reward-related behaviour

(water reward upon pressure of a lever), hence corroborating our findings relating GP to

saliency components of the task. This view is in line with recent evidence in favour of an

extension of GPe concept from its well-known 'relay station' role within the indirect

pathway, to a crucial function in the coordination of neuronal activity in the BG network

[97]. On the other hand, attempting to parse specific and exclusive pathways within the BG is

likely not the optimal approach given the high level of intra-connectivity patterns within

these nuclei [97]. Nevertheless, future investigations might benefit from a more in-depth

examination of the role of the subthalamic nucleus in such networks.

These proposed models provide a theoretical framework in favor of a flexible subcortical

modulation of top-down regulation of attentional allocation, which for the GP appears to be

specifically engaged in tasks involving value-saliency processing. Nevertheless, the

aforementioned possible modulatory routes should not be considered as mutually exclusive: a

more comprehensive model of attentional control should instead account for multiple cortical

and subcortical pathways operating in parallel, which would allow optimization of the

organism's interaction with the environment.

Materials and Methods

Participants

In the present study, we re-analysed the previously acquired dataset described in [38], where

twenty-eight healthy volunteers participated in the study (mean age: 23±2.7 years; 17 female;

all right handed). All participant reported normal or corrected-to-normal vision and no prior

knowledge of Chinese language. Of these, datasets from three participants were excluded

from the analysis (due to respectively: technical error during acquisition, excessive eye

movements during MEG recording and structural MRI data not acquired), leaving 25

participants. The experiment was conducted in compliance with the Declaration of Helsinki

and was approved by the local ethics board (CMO region Arnhem-Nijmegen,

CMO2001/095).

Experimental procedure

The experiment consisted of two phases: in the learning phase, participants were trained to

memorize associations between 6 Chinese characters and 3 different values (positive,

negative, neutral). Conditioning was implemented by means of visual and auditory feedback:

two symbols were associated with reward (+80 cents and a 'kaching' sound), two with loss (-

80 cents and a 'buzz' sound) and two with no value (0 cents and a 'beep' sound) (see Figure

1A for an example stimulus-reward association). The stimulus-reward pairing was

randomized across participants. Each trial started with the display of three fixation crosses

(1000ms), followed by the presentation of a Chinese character (1000ms), together with its

matching visual and auditory feedback (Figure 1B). Stimuli were displayed on a grey

background, each of them was presented twelve times in a randomized order. The learning

phase was conducted in a laboratory with attenuated sound and light and without MEG

recording. With the aim of reducing extinction, upon completion of this phase participants

were informed that the learnt stimulus-feedback associations would be signalling real reward

outcomes throughout the testing phase (i.e. the presentation of a Chinese character,

irrespective of its role as target or distractor, would result in a financial reward, loss or none).

After the learning phase, participants performed a testing phase (Figure 1C), when they were

required to perform a covert spatial attention tasks including the stimuli previously associated

with a monetary outcome, while ongoing electromagnetic activity was recorded with MEG.

In the testing phase, participants performed 8 blocks of 72 trials. Each trial started with the

presentation of three fixation crosses for 1000 ms (pre-trial interval), whose contrast

subsequently decreased, as a preparatory cue indicating imminent stimuli presentation. After

500ms, two symbols were presented to the left and right of the screen (8 degrees visual angle)

respectively, together with a central fixation cross flanked by two arrows, indicating the

target side. Participants were instructed to covertly attend the symbol on the cued side

('target') and to ignore the other one ('distractor'), until one of them changed contrast. The

contrast change either increased or decreased with equal probability, with onset after 750 ms

(13% trials), 1450 ms (47% trials, 'short interval trials') or 2350 ms (40%, 'long interval

trials') from stimulus presentation. Participants were asked to report the direction of the

contrast change at the targeted ('cued') location as quickly as possible by button press, using

the index or middle finger of the right hand to indicate their choice (finger-direction mapping

was randomized across participants). Participants were instructed to refrain from responding

when the distractor changed contrast. Shorter intervals of 750 ms were used to ensure that

participants would start covertly directing their attention rapidly after the cue; these trials

were not included in the analysis. The target changed contrast on 95% of the trials (valid

trials), whereas in the remaining trials the distractor did (invalid trials). The approximate

duration of the full task in the MEG was 50 minutes.

As a result of the conditioning manipulation in the learning phase, targets and distractors in

the task would be associated with either a salient (positive or negative) or a neutral value,

resulting in three categories of trials of interest, as represented by different levels of value-

salience, namely: zero (target and distractor neutral), one (target or distractor salient) or two

(target and distractor salient) value-salience levels.

MEG data acquisition

Electromagnetic brain activity was recorded from participants while seated, using a CTF 275-

channels whole-head MEG system with axial gradiometers (CTF MEG Systems, VSM

MedTech Ltd.). The data were sampled at 1200Hz, following an antialiasing filter set at

300Hz. Head position was constantly monitored throughout the experiment via online head-

localization software. This had access to the position of the three head localization coils

placed at anatomical fiducials (nasion, left and right ear), allowing, if necessary, readjustment

of the participant's position between blocks [98]. Horizontal and vertical EOG and ECG

electrodes were recorded with bipolar Ag/AgCl electrodes.

MEG data analysis

MEG data analysis was performed using the FieldTrip Toolbox running in MATLAB [99].

Continuous data were segmented in epochs, centred at the onset of the target contrast change,

encompassing the preceding 1500 ms and the following 200 ms (this way covering the full

stimulus presentation window for short trials). A notch filter was applied at 50, 100, 150 Hz

to remove line noise, the mean was subtracted and the linear trend removed. Automatic

artifact rejection was implemented for detection and removal of trials containing eye blinks

and horizontal eye movements (detected with EOG), MEG sensor jumps and muscle artifacts.

We produced virtual planar gradiometers by computing spatial derivatives of the magnetic

signal recorded with axial gradiometers [100]. The method has the advantage of improving

the interpretation of the topographic mapping since neural sources would produce a gradient

field directly above them. Time-frequency representations (TFR) of power were then

calculated for the resulting pairs of orthogonal planar gradiometers, before summing the

power values at each sensor. The analysis was performed by sliding a fixed time window of

500 ms in steps of 50 ms. The resulting data segments were multiplied by a Hanning taper

and a fast Fourier transform was applied in the $2 - 30Hz$ frequency range, in steps of 2Hz.

This procedure was applied only for correct valid trials, separately for left and right cued

conditions.

For each participant, TFRs were averaged across trials and a Modulation Index (MI) was

computed for each sensor k and over all time points t belonging to the time window of

interest -750 – 0 ms, according to the formula:

$$MI(f)_{k,t} = \frac{Power\ (f)_{k,t\ att\ right} - Power\ (f)_{k,t\ att\ left}}{Power\ (f)_{k,t\ att\ right} + Power\ (f)_{k,t\ att\ left}} \qquad \textbf{(1)}$$

Where $Power(f)_{k,t\ att\ left}$ represents the power at a given frequency f in the condition

'attend left' and $Power\ (f)_{k,t\ att\ right}$ is the power of the same frequency in the condition

'attend right'. As a result, positive (or negative) MI values, at a given sensor k and given

timepoint t, indicate higher power at a given frequency f when attention was covertly directed

towards the right (or left) hemifield.

Two clusters of sensors were then derived, by selecting the twenty symmetrical occipito-

parietal sensors (i.e. ten pairs of sensors) showing the highest interhemispheric difference in

alpha modulation indices, when considering the grand average over all conditions (see Figure

2A) averaged over the previously defined time window of interest. These clusters constituted

the regions of interests (ROIs) on which subsequent analysis was focused. Subsequently, in

order to quantify individual hemispheric-specific bias with respect to modulation indices in

the alpha range (MI(α)), we calculated the Hemispheric Lateralized Modulation (HLM)

index per participant:

$$HLM(\alpha) = \frac{1}{n_{right}} \sum_{k_{right}=1}^{n_{right}} MI(\alpha)_{k_{right}} + \frac{1}{n_{right}} \sum_{k_{left}=1}^{n_{left}} MI(\alpha)_{k_{left}} \qquad (2)$$

Where k_{left} and k_{right} denote sensors belonging to the aforementioned and previously

defined left and right clusters, respectively. Please note that $MI(\alpha)_k$ indices in Eq.2 (for both

k=1, ..., n_{right} and k=1, ..., n_{left}) are already a result of an average over timepoints of

interest t. Since MI(α) values were obtained by subtracting alpha power in 'attend left' trials

from 'attend right' trials, and given that, as a result of attentional allocation, alpha power is

suppressed in the hemisphere contralateral to the attended hemifield, a positive HLM(α)

value indicated that a given participant displayed higher modulation of absolute magnitude of

alpha power in the right compared to the left hemisphere, and vice versa (see Figure 2B).

Structural data acquisition

T1-weighted images of three out of twenty-five participants were acquired on a 3 T MRI

scanner (Magnetom TIM Trio, Siemens Healthcare, Erlangen, Germany), acquisition

parameters: TR/TE= 2300/3.03 ms; FA=8°; FoV= 256 × 256 mm; slice thickness= 1 mm;

Acquisition matrix= 0×256×256×0. For the remaining participants, a 1.5T MRI scanner was

used (Magnetom AVANTO, Siemens Healthcare, Erlangen, Germany). Acquisition

parameters: TR/TE= 2250/2.95 ms; FA=15°; FoV= 256 × 256 mm; slice thickness= 1 mm;

Acquisition matrix= 0×256×256×0.

Analysis

Structural analyses were conducted using the Integrated Registration and Segmentation Tool

(FIRST) within FMRIB's Software Library (FSL) v5.0.9 (www.fmrib.ox.ac.uk/fsl/, Oxford

Centre for Functional MRI of the Brain, Oxford, UK). A standard 12 degrees of freedom

affine registration to MNI152 space was applied to individual T1 images, adjusted with

optimal sub-cortical weighting. Bayesian models implemented in the software are derived

from a training based on previous manual segmentation of 336 datasets (provided by the

Center for Morphometric Analysis (CMA, MGH, Boston) and applied to registered images to

extract subcortical volumetric outputs for left and right hemispheres (see Figure 3A).

Given the reward components of the task we then focused on regions of the basal ganglia

identified by the algorithm namely the Globus Pallidus (GP), Nucleus Accumbens (Acb),

Caudate (CN), Putamen (Pu), as well as other regions potentially involved in the

mechanisms, namely Hippocampus (Hpc), Amygdala (Am) and Thalamus (Th). To compute

hemispheric Lateralized Volume indices (*LV*) for each substructure of interest *s*, we used the

following formula, which controls for individual differences in specific subcortical volumes

via normalization by total bilateral volume, commonly employed to evaluate structural brain

asymmetries [34,39]:

$$LV(s) = \frac{V(s)_{right} - V(s)_{left}}{V(s)_{right} + V(s)_{left}} \qquad (3)$$

Where $V_{S_{right}}$ and $V_{S_{left}}$ represent respectively the anatomical right and left volumes (in

voxels) for a given substructure s. Analogously to Eq.(2), a positive (or negative) LV_S index,

in a given participant, indicated a greater right (or left) volume for a given substructure s (see

Figure 3B).

Statistics

Generalized Linear Model

In order to determine the relationship between Basal Ganglia Lateralized Volumes (LV_S) and

electromagnetic indices (HLM(α)) we applied a generalized linear regression model (GLM),

specifying subcortical volumes lateralization (LV_s values) as regressors and individual HLM

values as the response vector, according to the formula:

$$HLM(\alpha) \sim \beta_0 + \beta_1 LV_{GP} + \beta_2 LV_{NAcc} + \beta_3 LV_{CN} + \beta_4 LV_{Pu} + \beta_5 LV_{HPC} +$$
$$\beta_6 LV_{Am} + \beta_7 LV_{TH} + \varepsilon \qquad (4)$$

600 All subsequent analysis on the relationship between volumetric and oscillatory data

601 specifically focused only on the subcortical structure(s) associated with a significant β

602 coefficient in the model in Eq.(4), below referred as LV_s.

Cluster based permutation test

To evaluate whether the linear association between LV_s and HLM was effectively limited to the alpha band, a cluster based permutation approach [41] was employed over the full time frequency spectrum of interest. This method effectively allows to statistically control for multiple comparisons over all time and frequency points of interest. After selecting the *a-priori* sensors belonging to the formerly specified ROIs, we considered a permutation distribution of regression coefficients derived from randomly pairing participants' LV_s value (independent variable) and modulation indices (HLM(f)) 1000 times. At every time-by-frequency point, the actual regression coefficient was evaluated against the aforementioned distribution by means of a specified critical α value. Afterwards, a time-frequency map of the cluster level statistics was derived showing sets of sensors associated with a significant effect.

An equivalent approach was later applied to investigate possible hemisphere-specific differences in alpha modulation between participants showing a right or left lateralized substructure s. Directionality of lateralization was determined by median split of the distribution of LV_s per participant, producing two subgroups of N=12, representing subjects with a larger left or right volume of substructure s. After having a-priori averaged across the time-frequency spectrum of interest ([-750 0] ms, 8-13Hz), MI(α) values at every sensor were compared between the two subgroups (right vs left lateralized substructure). The actual t-value was then compared with a permutation distribution of t-statistic derived from randomly partitioning indices between the two groups 1000 times. As a result, a topography map was plotted displaying eventual cluster(s) of sensors associated with a significant t-value (i.e. a significant difference in MI(α) between subgroups).

 Comparison between Pearson's correlation coefficients

Finally, we aimed at comparing the association between the derived structural and functional

lateralization indices in different value salience occurrences. To this end, we calculated

HLM(α) values for each participant separately for the three reward-related contingencies and

computed the Pearson's correlations with LV_S indices which displayed a significant β as

arising from the model in Eq.(4). We statistically assessed the difference in correlation

coefficients between the three experimental conditions considered, according to the method

described in [101]. The test implements a percentile resampling technique by generating a

bootstrap sample of the difference of the correlation coefficients between the overlapping

variable LV_{GP} (Y) and the two variables representing the HLM(α) for the two experimental

conditions (VO levels) to be compared (X_1, X_2). As suggested in the method, we used a

Winsorized correlation to achieve a robust measure of association between variables. This

transformation has been shown to effectively control for the influence of outliers on the

correlation estimate [102]. A confidence interval was then computed on the resulting

bootstrap distribution, to assess the statistical significance of the actual difference between

correlation coefficients describing the different VOs.

Behavioural data analysis

To assess whether subjects displayed a spatial bias during the task, we first averaged across

left and right cued trials separately, averaged across all conditions (i.e., irrespective of value-

saliency occurrences (VO)). We then employed paired t-test on the derived reaction times

(RT) and accuracy (ACC) (expressed as percentage of correct responses) measures for the

left and right cued trials. Secondly, we divided trials according to VO pairings, averaging left

and right cued trials, to determine whether behavioural performance varied as a function of

saliency in both RT and ACC. We here employed one-way repeated measures ANOVA to

assess whether group means in the three conditions significantly differ from each other. We

also considered individual lateralized measures of RT and ACC across different VO

conditions. To this end, behavioural asymmetries in performance (BA) for both measures

were calculated according to:

$$BA_{RT/ACC} = \frac{BA_{RT/ACC_{right}} - BA_{RT/ACC_{left}}}{BA_{RT/ACC_{right}} + BA_{RT/ACC_{left}}} \tag{5}$$

Where $BA_{RT\,right}$ and $BA_{RT\,left}$ represent mean reaction times for 'attend right' and 'attend left'

trials, respectively. A positive BA_{RT} for a given subject indicated faster responses when a

participant was validly cued to the left compared to the right hemisphere, while negative

values indicated the opposite pattern. Consequently, positive BA_{ACC} values indicated higher

accuracy on 'attend right' trials compared to 'left attend' trials, and vice versa.

A one-way repeated measures ANOVA was employed to test the difference across group

means in the three VO conditions examined.

In a next step, we sought to investigate the possible association of behavioural performance

with structural and functional hemispheric lateralization, we used Pearson's correlation to

examine the association of individual asymmetries in accuracy (BA_{ACC}) and reaction times

(BA_{RT}) with individual HLM(α) and LV values of subcortical structures which showed

significant correlation with HLM(α).

In a last step, we employed a general linear model (GLM) in order to assess whether spatial

biases in behavioural performance could be explained by a combination of the other

variables, namely HLM(α) and the LV indices of the subcortical areas considered, according

to the formula:

$$BA_{RT/ACC} \sim \beta_0 + \beta_1 LV_{GP} + \beta_2 LV_{NAcc} + \beta_3 LV_{CN} + \beta_4 LV_{Pu} + \beta_5 LV_{HPC} +$$

$$\beta_6 LV_{Am} + \beta_7 LV_{TH} + \beta_4 HLM(\alpha) + \varepsilon$$

(6)

Data availability

The preprocessed MEG and MRI anonymised dastasets that support the findings of this study

are available as downloadable online data collection in the Donders Data Repository

(https://data.donders.ru.nl), with persistent identifier: 11633/di.dccn.DSC_3016045.01_337,

upon reasonable request to the corresponding author.

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A

Positive   Negative   Neutral

Salient

B

Fixation
1000ms

Stimulus
♪ 'Kaching!'
1000ms

Fixation
1000ms

Stimulus
♪ 'Buzz!'
1000ms

C

Pretrial Interval
1000ms

Preparatory Cue
500ms

Stimuli Presentation
1450 - 2350ms

Contrast Change
1000ms

Figure 1. Illustration of selective attention task: stimuli and reward manipulation.

(A) Six Chinese symbols served as stimuli for the task and were associated with three values: two paired with reward, two with loss and two with no financial change (neutral). (B) Representative trial of the learning phase. Symbols were displayed for 1000ms, systematically paired with the corresponding (positive, negative or neutral) value, via visual and auditory feedback. Characters presentation was alternated with a 1000ms fixation period. During the training phase, participants learned associations between the stimuli and their reward value. **C.** Representative trial of the testing phase. After a 1000ms pretrial interval, participants were primed with a 500ms preparatory cue signalling the upcoming stimuli. Two characters were then presented to the left and right hemifield, together with a spatial cue, instructing participants to covertly attend the symbol on the cued side (target) and ignore the other one (distractor). Participants' task was to report when the target stimulus changed contrast. Contrast change could either occur after 750ms (13% of trials), 1450ms (47% of trials) or 2350ms (40% of the trials). In 95% of the trials, the target changed contrast (valid trials), whilst in 5% of the trials, the distractor changed contrast (invalid trials). Figure adapted from [38].

Figure 2. Grand average MI and HLM distribution across participants.

(A) Time-frequency representations of power (TFRs) and topographical plot showing contrast between the 'attention right' – 'attention left' trials. A clear modulation is visible at posterior sensors in the alpha band (8 – 13Hz) in the –750 – 0ms interval (this time window being considered for the computation of HLM(α) indices in (B)). Sensors included in the left and right ROIs are marked as dots. Trials are locked to the onset of the contrast change (t = 0). (B) Side panels show the temporal evolution of modulation indices in the alpha range (MI(α)), averaged over sensors within left and right hemisphere ROIs. The magnitude (absolute value) of MI(α) progressively increased in the stimulus interval until the onset of the contrast change. Middle: distribution of HLM(α) indices across participants, computed over the ROIs and 8 – 13 Hz frequency band (see Materials and Methods). A normal density function is superimposed, denoting no hemispheric bias in lateralized modulation values across participants (Shapiro Wilk, W = .958, p = .392).

Figure 3. Basal Ganglia volumes resulting from semiautomated subcortical segmentation implemented.

(A) Orthogonal view and 3D rendering. Subcortical volumes are overlaid as meshes on the anatomical MRI of one of the participants (following defacing procedure in Freesurfer, where voxels outside the brain mask with identifiable facial features were excluded [103]). (B) Histograms with superimposition of normal density function, showing the distribution of subcortical lateralization indices for each substructure. In our sample, NAcb and Th volumes were left lateralized (p = .0001 and p=.0003, respectively) while CN showed a right lateralization (p = .0029).

Figure 4. Lateralization of individual subcortical structures in relation to alpha hemispheric lateralized modulation (HLM) in the task. (A) Bar plot displays the Beta coefficients associated with a general linear model where LV values were defined as explanatory variables for HLM(α). Error bars indicate standard error of the mean. Asterisks denote statistical significance; **p < .01. (B) Partial regression plot showing the association between LV_{GP} and HLM(α), while controlling for the other regressors in the model in (A). (C) Partial regression plot showing the association between LV_{Th} and HLM(α), while controlling for the other regressors in the model in (A). Given Eqs.(1) and (2) (see *Materials and Methods*), positive HLM(α) values indicate stronger modulation of alpha power in the right compared to the left hemisphere, and vice versa; similarly, positive (or negative) LV_s indices denote greater right(or left) volume for a given substructure *s*. The dotted curves in (B) and (C) indicate 95% confidence bounds for the regression line, fitted on the plot in black.

Figure 5. Time-frequency representation of regression coefficient t-statistics on the linear relationship between lateralized

alpha modulation and LV_{GP} (A) and LV_{Th} (B) indices, averaged over ROIs (see Fig. 2A). A black outline is used to highlight

the significant time-frequency cluster found. For the LV_{GP}, the analysis revealed a clear α-band-limited association between

the variables across the full time-window of interest (see *Materials and Methods*).

Figure 6. Linear association between GP volumetric asymmetry and alpha modulation asymmetry as a function of

value-saliency occurrences in the task. (A) Correlation between GP volume lateralization and HLM(α), grouped accordingly

to the number of value-salient stimuli in the trials (see *Materials and Methods*). From left to right, respectively, two, one and

zero value-saliency occurrences are displayed. GP asymmetry significantly explained HLM(α) only when value-salient stimuli

featured as both target and distractors, irrespective of their valence ($r = .68$, significant at the $p < .001$ level after Bonferroni

correction for three comparisons). (B) The association between HLM(α) and GP volume lateralization increased as a function

of value saliency in the task: the linear relationship was stronger when two value-salient stimuli were presented, when

compared to conditions characterized by either one or value-salience pairings (95% CI [.106, .672] and [.125, .897],

respectively for the two comparisons). This suggests that, when both target and distractor were associated with a salient value,

participants exhibiting bigger GP volume in the left hemisphere than in the right hemisphere, were also better at modulating

alpha oscillations in the left compared to the right hemisphere. Asterisks denote statistical significance; **$p < .01$.

Figure 8. Mean and lateralized reaction times (RT) and accuracy values across the three value-saliency occurrences in the task.

Mean RT (A) and accuracy (C) values averaged across participants in the three value-salient occurrences conditions in the task. Error bars indicate standard error of the means. No significant difference was found between groups by means of one-way repeated measures ANOVA, indicating that different levels of value-saliency pairings didn't influence behavioural performance. No significant difference emerged also when comparing average lateralized values of RT (B) and accuracy (D) across the same conditions, and by means of same statistical analysis, indicating that the behavioural spatial bias was not affected by the different levels of value-saliency pairings.

1059 **Supplementary material**

1060

Figure 1S. Alpha modulation indices for left and right hemispheres associated with two subgroups of the sample. (A)

Topographical plot of MI(α) values for the two participants groups, clustered according to directionality of GP lateralization

(right vs left lateralized GP). Left and right sensors of interest are marked as dots and correspond to the same ROIs as in

Figure 2. (B) Bar graph showing mean MI(α) averaged over ROIs in the two subgroups. As indicated in the cluster-based

permutation results, a difference is particularly observable for right hemisphere alpha modulation between the two groups,

being higher in participants exhibiting a right lateralized GP. Error bars represent standard error of the mean. Horizontal

lines in the indicate the average HLM(α) indices for each subgroup.

A

B

1068   **Figure 2S**. General linear model displaying combined lateralized subcortical volumes and hemispheric lateralized

1069   modulation as multiple regressors for the prediction of spatial behavioural bias in accuracy (A) and RT (B). No significant

1070   regression was found which could account for either the lateralized accuracy or RTs ($p=.429$ and $p=.570$, respectively).