Interactions between microtubule-driven membrane protrusions induce filament bundling

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⁴ Keywords: cytoskeletal-membrane interactions, filament bundling.

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Abstract

⁶ The plasma membrane and cytoskeleton of living cells are closely coupled dynamical systems.

 $_{7}\,$ Internal cytoskeletal elements such as actin filaments and microtubules continually exert

 $_{\ensuremath{\mathfrak{s}}}$ forces on the membrane, resulting in the formation of membrane protrusions. In this paper

⁹ we investigate the interplay between the shape of a cell distorted by pushing and pulling forces

¹⁰ generated by microtubules and the resulting rearrangement of the microtubule network.

¹¹ From analytical calculations, we find that two microtubules that deform the vesicle can ¹² both attract or repel each other, depending on their angular separations, the size, and the

¹² both attract or repel each other, depending on their angular separations, the size, and the ¹³ direction of imposed perturbations. We likewise find the necessary conditions for attractive

¹⁴ interactions between multiple microtubules. Our results suggest that the commonly reported

¹⁵ parallel structures of microtubules in both biological and artificial systems can be a natural

¹⁶ consequence of membrane mediated interactions.

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17 Introduction

Cells are enveloped by a plasma membrane which serves as a selective soft physical bar-18 rier as well as being home to many functional proteins. The stability and shape of cellular 19 membranes are determined not only by inherent properties of the membrane, but also by 20 interactions with the cell's cytoskeleton (1). The highly dynamic cytoskeletal network is 21 vital for numerous biological processes, including cell motility, cell migration, and cell sig-22 naling (2, 3). A typical feature occurring in such processes is the formation of membrane 23 protrusions. Protrusions commonly emerge in the form of microvilli, filopodia or lamellipo-24 dia (4, 5). These leading-edge protrusions, the existence of which is vital for responding to 25 external cues, can be driven, controlled and elongated by a complicated crosstalk between 26 the membrane and underlying filaments. 27

- The spatial arrangement of cytoskeletal filaments, force generation mechanisms, and cy-28 toskeletal networks coupling to the shape of cells have been investigated extensively, both 29 theoretically and experimentally (6–10). For example, when growing encapsulated micro-30 tubules inside an artificial spherical membrane, it has been shown that the vesicle exhibits 31 a diverse range of morphologies, from a simple elongated shape to dumbbell-like geometries 32 (7). The diversity in the shape of such vesicles results from both the elongation dynamics of 33 the filaments inside them and the material properties of the membrane. Such spatial rear-34 rangement of filaments does not occur spontaneously but stems from the conditions imposed 35
- ³⁶ on them from various elements, one of which is the cell shape.
- ³⁷ In this paper, we investigate the interplay between the shape of vesicles, that are deformed
- by internal force generating filaments like microtubules, and the rearrangement of those fil-38 aments. In a biological cell, microtubules undergo treadmilling and dynamic instabilities 39 (catastrophes) which are controlled by associated proteins (11). Only a few of the micro-40 tubules that grow inside a cell can reach the cell membrane (12). The pushing and pulling 41 forces generated by those few microtubules can be harnessed for creating protrusions of the 42 membrane (13). Membrane mediated interactions between microtubule-induced protrusions 43 may influence the arrangement of other functional filaments in addition to microtubules 44 themselves (14, 15). Therefore, it is warranted to study how the presence of a biological 45 membrane, which has both elastic and fluid properties, alters the interaction between micro-46 tubules. This interaction could both drive processes like the formation of filament bundles 47
- 48 or inhibit microtubule aggregation.

We use a modified version of the theoretical framework that has been developed for investi-49 gating membrane mediated interactions between proteins embedded in or bounded to a fluid 50 membrane (16, 17). We first explain the model in detail. We then study the effects of all the 51 possible elements on the interaction between microtubules. In particular, we demonstrate 52 that changing the in-plane tension in the membrane qualitatively affects the equilibrium 53 shape that a vesicle can adopt. We further reveal that the size and relative orientation 54 of the imposed deformations determines the nature of their interactions. Our results thus 55 elucidate the effective role of the membrane in determining the equilibrium arrangement of 56 protrusions imposed by the cytoskeleton. 57

58 Model

⁵⁹ We assume that microtubules (including their tip) are rigid and impose sharp deformations ⁶⁰ on the membrane. To analyze the effect of such perturbations on the shape of an undeformed ⁶¹ spherical membrane, we use the conventional Canham-Helfrich bending free energy including ⁶² fixed surface area (S) and volume (V) constraints, given by:

$$E_{\rm CH} = \int dS \left[2\kappa H^2 + \sigma \right] + \Delta P \int dV \tag{1}$$

with H, σ and ΔP the sum of the two principal curvatures, surface tension and pressure difference, respectively. Due to the conservation of topology we can ignore the Gaussian curvature contribution in the energy functional. Using the spherical analog of the Monge parametrization, we describe the shape of a deformed vesicle as:

$$r(\theta, \phi) = R\left(1 + u(\theta, \phi)\right) \tag{2}$$

where R is the radius of an undisturbed vesicle and $u(\theta, \phi)$ is the deformation field. As the only constraints present are those imposed by the microtubules, we fix the amount of induced deformation at their tip (Fig. 1), $\bar{\mathbf{u}}_0 = (u(\theta_1, \phi_1), \dots, u(\theta_N, \phi_N))$ with N the number of microtubules. Mathematically, we apply this condition via Lagrange multipliers,

$$E_{\rm MTs} = \int dS \left[\mathbf{L} \cdot \left(\bar{\boldsymbol{\delta}} (\Omega - \Omega_0) u(\theta, \phi) \right) \right], \text{ where } \bar{\boldsymbol{\delta}} (\Omega - \Omega_0) = \begin{bmatrix} \delta(\Omega - \Omega_1) \\ \cdot \\ \cdot \\ \delta(\Omega - \Omega_N) \end{bmatrix}$$
(3)

where **L** is a vector of Lagrange multipliers and $\delta(\Omega - \Omega_i) = \delta(\cos(\theta - \theta_i)) \delta(\phi - \phi_i)$ is the Dirac delta function for spherical coordinates. In terms of the deformation field and the applied constrains, the total energy of the membrane is given by:

$$\frac{E_{\text{Total}}}{\kappa} = \int d\Omega \left[2\left(1 - \nabla^2 u + \frac{1}{4}(\nabla^2 u)^2 + u\nabla^2 u + \frac{1}{2}|\nabla u|^2\right) + \bar{\sigma}\left((1+u)^2 + \frac{1}{2}|\nabla u|^2\right) - \frac{\overline{\Delta P}}{3}(1+u)^3 - \mathbf{L} \cdot (\bar{\boldsymbol{\delta}}u) \right],$$
(4)

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where the nondimensionalized surface tension and pressure difference are defined as $\bar{\sigma} = \frac{R^2 \sigma}{\kappa}$ and $\overline{\Delta P} = \frac{R^3 \Delta P}{\kappa}$, respectively. In the small deformation regime, we can approximate the relative behavior of the pressure difference and surface tension as that of the Laplace pressure for a sphere: $\overline{\Delta P} = 2\bar{\sigma}$. We then obtain the linearized form of the shape equation by minimizing Eq. 4, which gives:

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$$\nabla^2 \nabla^2 u + (2 - \bar{\sigma}) \nabla^2 - 2\bar{\sigma} u = \mathbf{L}.\bar{\boldsymbol{\delta}}$$
(5)

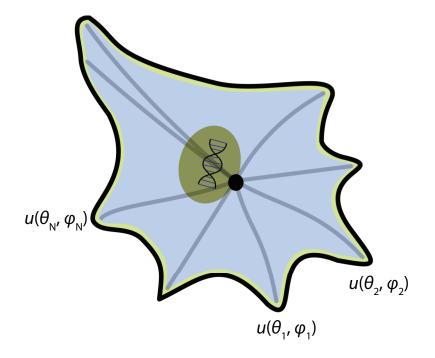


Figure 1: Schematic shape of a cell containing some microtubules. We model the microtubules by the imposed deformation $(\bar{\mathbf{u}}_0 = (u(\theta_1, \phi_1), \dots, u(\theta_N, \phi_N)))$ at their tips.

Because the resultant equation is linear, the final solution for the deformation field of the membrane can be constructed as:

$$u(\theta, \phi) = \mathbf{L} \cdot \bar{\mathbf{g}}(\Omega - \Omega_0), \text{ where } \bar{\mathbf{g}}(\Omega - \Omega_0) = \begin{bmatrix} G(\Omega - \Omega_1) \\ \cdot \\ \cdot \\ G(\Omega - \Omega_N) \end{bmatrix}.$$
(6)

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⁹⁰ In these equations $G(\Omega - \Omega_i)$ is the Green's function of the left hand side of Eq. 5. We ⁹¹ expand the Dirac delta function in terms of spherical harmonics¹, and solve for the Green's ⁹² function, which gives:

$$G(\theta - \theta', \phi - \phi') = \sum_{l=2}^{\infty} \sum_{m=-l}^{l} \frac{Y_l^m(\theta, \phi) Y_l^{m*}(\theta', \phi')}{l^2(l+1)^2 - (2 - \bar{\sigma})l(l+1) - 2\bar{\sigma}}.$$
(7)

In Eq. 7 we have excluded the first two modes. The zeroth mode corresponds to motion of the center of mass. Excluding the first mode is necessary to prevent inflation of the vesicle, as we have already penalized any changes in the volume in Eq. 4. Excluding these modes implies correcting the Dirac delta in Eq. 5, which is reasonable for small deformations. Finally, taking into account the constraints associated with the microtubules (the vector $\bar{\mathbf{u}}_0$),

 $[\]overline{1\delta(\phi - \phi')\delta\left(\cos\left(\theta - \theta'\right)\right)} = \sum_{l=0}^{\infty} \sum_{m=-l}^{l} Y_l^m(\theta, \phi) Y_l^{m*}(\theta', \phi'), \text{ where the symbol `*' denotes complex conjugate.}$

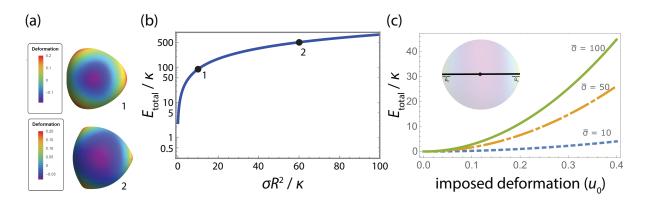


Figure 2: Membrane deformation due to the presence of microtubules. (a) Snapshots of a deformed vesicle for low (1) and high (2) values of the surface tension. The imposed deformation vector reads $\bar{\mathbf{u}}_0 = (0.1, 0.1, 0.1)$. (b) Increasing the in-plane tension makes the membrane deformation more spiky, in contrast to low surface tension regimes where we have rounded deformations. Numbers correspond to the images in (a). (c) The deformation energy of a spherical membrane containing two growing microtubules for different values of the surface tension.

⁹⁹ we obtain the Lagrange multipliers and the induced deformation field as:

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$$\mathbf{L} = \bar{\mathbf{u}}_0^T \cdot \mathbf{M}^{-1}, \text{ and } u(\theta, \phi) = \bar{\mathbf{u}}_0^T \cdot \mathbf{M}^{-1} \cdot \bar{\mathbf{g}}(\Omega - \Omega_0),$$
(8)

where **M** is an $N \times N$ matrix whose components are constructed as $m_{ij} = G(\theta_i - \theta_j, \phi_i - \phi_j)$, with i = 1, ..., N and j = 1, ..., N. For the diagonal components of the matrix **M** (when i = j, corresponding to self-interactions), because we have a constant number of lipids and the vesicle is closed, we consider a maximum mode $l = L_{\text{max}}$ in Eq. 7. Substituting the derived deformation field $u(\theta, \phi)$ in Eq. 4, one can get the total energy of the membrane as:

$$\frac{E_{\text{Total}}}{\kappa} = \frac{1}{2} \bar{\mathbf{u}}_0^T \cdot \mathbf{M}^{-1} \cdot \bar{\mathbf{u}}_0 + 8\pi \left(1 + \frac{\bar{\sigma}}{3}\right).$$
(9)

Given an arbitrary number of microtubules, all we need is the amount of deformation they impose to investigate their interactions. The only relevant length scale of our system relates surface tension to the bending modulus, given by $\lambda = \sqrt{\kappa/\sigma}$. In a biological context, the pertinent values of λ are in the range of 60 - 100 nm (18, 19). Given this length scale, one can obtain the nondimesionalized physiologically relevant values of surface tension as: $\bar{\sigma} = (R/\lambda)^2$. For a value of $\lambda = 100$ nm, for example, we get $\bar{\sigma} = 100$ for a vesicle size of $R = 1 \ \mu$ m.

To examine the effect of surface tension on the equilibrium shape of the membrane, we position three microtubules inside a vesicle such that they form an equilateral triangle, and all impose the same amount of deformation on the membrane ($u_0 = 0.1$). For small values of $\bar{\sigma}$, we are in a bending dominated regime. The membrane, therefore, minimizes the total mean curvature, as illustrated in Fig. 2a. Increasing $\bar{\sigma}$ alters the local shape of membrane

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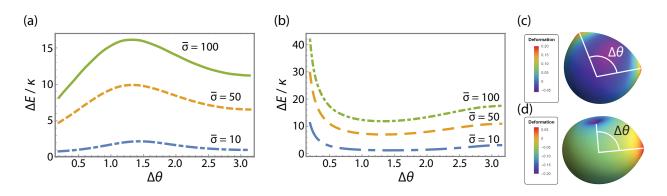


Figure 3: The interaction between microtubule-driven protrusions. (a) Microtubules that deform the membrane identically, attract each other and bundle for separations smaller than a critical angle $\Delta \theta_c \simeq 5\pi/12$. The elastic nature of the membrane hinders microtubule coalescence for larger separations. (b) Protrusions of opposite orientation repel each other for small distances and attract for large angular separations. Right panel: Snapshots of two protrusions that are imposed either identically (c) or oppositely (d).

at the tip of microtubules from being smoothly curved into sharp spikes with higher total 119 energy (Fig. 2b). Next, we analyze the total energy of a vesicle encapsulating two growing 120 microtubules that push the membrane in opposite directions (Fig. 2c). We assume that the 121 two microtubules distort the membrane similarly. As expected, the more a vesicle elongates, 122 the larger the stored energy becomes. Also, membrane vesicles with a high in-plane tension 123 require more energy to initiate a protrusion process. Microtubules are dynamic entities and 124 constantly switch between growing and shrinking phases that are characterized by rescue 125 and catastrophe events (20). Not only are they able to generate a pushing force during 126 growing into obstacles like membrane, microtubules can also release a force in the course 127 of shrinking, which can be harnessed for pulling purposes (in case of deformable obstacles). 128 The pushing forces are in the range of 2-3 pN (21), leading to an energy of $40-60 \kappa$ 129 for a deformation² of $u_0 = 0.1$. Therefore, having membrane protrusions that cost a total 130 energy (E_{Total}) of not more than $60 - 100 \kappa$ would still allow tubulin dimers to aggregate 131 at the end of the microtubules. The depolymerization-dependent forces are about one order 132 of magnitude stronger (~ 30-65 pN (22)) than those generated during the growth state. 133 Therefore, the force numbers in the biological context are high enough to impose distortions 134 of a similar size as we suppose in our calculations – although depending on the length of the 135 microtubules, some processes like buckling may decrease the maximum force they exert on 136 the membrane. 137

The arrangement of filaments plays a key role in the emergent shape of protrusions and consequently in sensing the extracellular environment. To unravel the nature of elastic interaction between protrusions, we investigate a vesicle containing two protrusions with a varying angular separation between them. For identical deformations, as illustrated in Fig. 3, we have both short-range attraction and long-range repulsion regimes, that are

²We assume a bending modulus of $\kappa = 25k_{\rm B}T$ for the membrane and a vesicle size of 1 μ m.

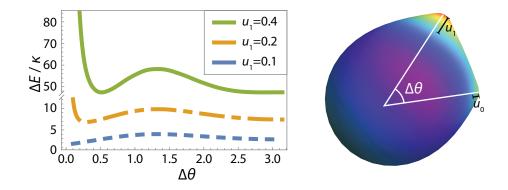


Figure 4: Interaction between microtubule-driven protrusions of different strength. As shown in the graph, introducing a difference in the magnitude of the protrusions results in a very strong short range repulsion between them $(u_0 = 0.1; \bar{\sigma} = 10)$.

connected at a critical angle $\theta_{\rm c} = 5\pi/12$. The plot suggests that cellular membranes facilitate 143 the aggregation of microtubules for short separations and hinder their assembly for longer 144 distances. Although the global minimum of the energy is when two protrusions are merged, 145 there is an energy barrier, the value of which increases with the surface tension. Inversely, 146 two oppositely oriented protrusions repel each other for short and attract for larger distances. 147 When analyzing the interaction between protrusions of different sizes, we realize that altering 148 the magnitude of deformation for one of the microtubules strikingly changes the nature 149 of interactions in their small separations. For example, as illustrated in Fig. 4, making 150 one of the constraints stronger/weaker than the other turns short range attraction into 151 repulsion. This suggests that having such distortions on a vesicle is costly, and that cells 152 will therefore try to minimize the amount of deformed material between them by adjusting 153 their protrusions. Putting the results of the two previous experiments together, we find that 154 when interacting with membranes, microtubules rearrange themselves in such a way to form 155 parallel filaments. Such rearrangements are ubiquitous in cells, for instance in the early 156 stages of filopodia. Our results therefore suggest that these phenomena can be a natural 157 result of membrane mediated interactions between microtubules. 158

Our system easily extends to vesicles that contain more than two microtubules, with similar results. To illustrate this point, we plot the whole configuration space for the case of three microtubules (Fig. 5) to look for the possible (semi) stable configurations. It turns out that the global minimum of the resultant energy landscape is when all the microtubules are attached to each other. There are, however, some local minima, all of which correspond to the situation where two microtubules are bundled together and the other points to the opposite pole of the vesicle.

166 Conclusion

¹⁶⁷ Together with actin and intermedediate filaments, microtubules form an architecture that ¹⁶⁸ governs the shape of a cell, and therefore that of the plasma membrane surrounding it. The

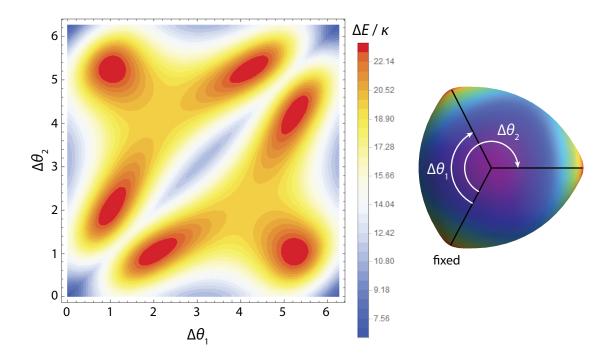


Figure 5: Plot of the configuration space of a vesicle with three enclosed microtubules, with the energy of each configuration shown in color. The closed shape of the vesicle favors the formation of parallel structures of microtubules. The global minimum of the energy corresponds to the situation where all the filaments are bundled, with local minima for the case of having two tubules together and one pointing in the opposite direction. Because filaments polymerize from the centrosome in opposite directions, the local minima may be biologically relevant.

membrane, in turn, mediates the interaction between attached microtubules. Using analyt-169 ical tools, we studied the effect of membrane mediated interactions on the rearrangement of 170 microtubules. Our results suggest that the elastic properties of cellular membranes facili-171 tate the bundling of microtubules. In particular, we showed that two vesicle-encapsulated 172 microtubules attract each other for small angular separations and repel for large angles. As 173 we explicitly demonstrated for three microtubules, the outcome of collective interactions be-174 tween multiple filaments is microtubule coalescence, which may be harnessed for protrusion 175 formation (23). Our results reveal that force generating microtubules, when colliding with a 176 deformable obstacle like a fluid membrane, can coordinate their growing state through the 177 shape of distorted membrane between them. Putting all the results together, our study sug-178 gests a possible mechanism underlying the preference of filaments for organizing in parallel 179 configurations (24). 180

Acknowledgments

This work was supported by the Netherlands Organisation for Scientific Research (NWO / OCW), as part of the Frontiers of Nanoscience program.

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