Evidence of ventral stream computations in rat lateral extrastriate

cortex

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Abstract

In rodents, the extrastriate areas located laterally to primary visual cortex (V1) have been assigned to a putative object-processing pathway (homologous to the primate ventral stream), based on anatomical considerations. Yet, functional evidence supporting this attribution is sparse. Here, we probed the specialization for ventral processing of rat laterolateral area (LL), located at the apex of the putative ventral-like hierarchy. To this aim, we recorded neuronal responses in both V1 and LL during presentation of drifting, oriented gratings and noise movies. We found that the degree of non-linearity of the stimulus-response relationship increased from V1 to LL, along with the tendency of neurons to respond to multiple orientations, while the sharpness of orientation tuning decreased. Critically, all these trends matched the predictions derived from a well-established model of ventral computations and from a meta-analysis of the monkey literature, thus reaffirming the specialization of LL for higher-order processing of shape information.

Introduction

In rats and mice, primary visual cortex (V1) is bordered by at least 9 extrastriate visual areas, whose involvement in dorsal and ventral stream processing (i.e., extraction of, respectively, motion and shape information[1,2]) has become the object of intense investigation[3–8]. To date, most studies on this front have been inspired by the segregation of visual information in the specialized channels[9] that, in primates, selectively relay low temporal/high spatial frequency signals (P-channel) to the ventral stream only, and high temporal/low spatial frequency content (M-channel) to both the ventral and dorsal streams[10,11]. Inspired by a possible homology with primates, several investigators have mapped mouse visual areas with drifting gratings of various spatiotemporal frequencies[12–18], finding the signature of dorsal processing

in medial and parietal extrastriate cortex, but only scant evidence of ventral computations in

lateral extrastriate regions. On the one hand, the validity of this approach is supported by the

existence of distinct neuronal subpopulations within V1, displaying either M- or P-like tuning

and making (receiving) target-specific projections with (from) downstream and upstream

areas[12,15,19,20]. On the other hand, tracking the routing of spatiotemporal information across

visual cortex does not take into account how local computations sculpt the tuning of visual

neurons within each area[8] – a process that is expected to play a dominant role especially in

the ventral stream, where the specialization for the processing of visual objects can only

emerge as the result of local, non-linear integration of presynaptic inputs from upstream

areas[21–23].

To find the signature of such computations, we recently tested how visual objects are

represented along rat lateral extrastriate areas[24]. Our experiments showed that neuronal

populations along this areas' progression become increasingly capable of supporting

discrimination of object identity despite transformations in object appearance (e.g., due to

translation and scaling), with the largest transformation tolerance achieved in the most ventral

region: the laterolateral area (LL). This trend matches very closely the key property of a

ventral-like pathway[21], thus strongly supporting the central role of LL in ventral processing.

At the same time, studying cortical representations of visual objects has the disadvantage of

relying on idiosyncratic choices of the stimulus set (the object conditions) and rather complex

interpretive approaches (e.g., information theory and machine learning). This makes the

experimental design hard to standardize, and often leads to conclusions that are only partially

overlapping across studies. The assignment of rat lateral extrastriate cortex to the ventral

stream is no exception, as shown by the much weaker specialization for object processing

found, in this region, by an earlier study[25].

This prompted us to verify the higher rank of LL, relative to V1, in ventral processing,

by designing an experiment that exploited the benefits of presenting parametric stimuli

(drifting gratings), but, rather than focusing on spatiotemporal tuning, measured the linearity

of the stimulus-response relationship – i.e., the extent to which a neuronal response can be

explained as a weighted sum of the stimulus intensity values within the neuron's receptive

field (RF). This property, which is the most discriminant of higher-order vs. lower-order

processing, was assessed by quantifying how locked the neuronal response was to the phase

of the gratings, thus distinguishing neurons with a linear, phase-sensitive behavior from

neurons with a non-linear, phase-invariant response. We complemented this analysis by

estimating the RF structure of the recorded units from their responses to noise movies using

the *spike-triggered average* (STA) method[26], and by examining the sharpness and shape of

their orientation tuning curves.

Critically, all these properties followed the trends of variations that are expected to

occur along the ventral stream, according to the predictions derived from a well-established

model of ventral computations and from a meta-analysis of the monkey literature. As such,

our results confirm the involvement of LL in higher-order processing of shape information,

and support the use of full-field parametric stimuli as a benchmark to screen rodent visual

areas for their implication in ventral processing.

Results

We used 32-channel silicon probes to perform extracellular recordings from areas V1 and LL

(Fig. 1a) of anaesthetized rats that were presented with drifting gratings of various

orientations, spatial (SF) and temporal (TF) frequencies, as well as with 80 30s-long movies

of spatially and temporally correlated noise (Methods). A total of 105 and 104 neurons were

recorded, respectively, from V1 and LL. With "neurons" we refer here to well-isolated single

units that were effectively and reproducibly driven by one or more of the grating stimuli

across repeated presentations (Methods). In addition to the main stimulus presentation

protocol, we also run a receptive field mapping procedure (Methods) to track the progression

of the RFs recorded along a probe (Fig. 1b). Given that, in rodents, the polarity of the

retinotopic map reverses at the boundary between each pair of adjacent visual cortical areas[8],

tracking the retinotopy of the RFs, combined with the histological reconstruction of the probe

insertion track (Fig. 1a), allowed a precise identification of the units that were recorded from

LL.

Fig. 1 Targeting rat laterolateral (LL) visual cortex for multi-electrode recordings using a

linear silicon probe. **a.** Representative Nissl-stained coronal slice showing the insertion track

of a single-shank silicon probe aimed at area LL. The probe was inserted obliquely into

visual cortex, crossing lateromedial (LM) and laterointermediate (LI) visual areas before

107 reaching LL. The dashed lines depict the borders of the areas, as reconstructed by tracking

108 the retinotopy of the receptive fields (RFs) recorded along the probe (see panel **b**). The

109 position of the probe during the recordings is marked by the staining with the fluorescent dye

110 (red) that was applied to it before insertion, and by the mechanical lesion produced by the

111 penetration. Based on this information, it was possible to estimate the geometry of the probe

112 (green lines) at the final recording depth (2.5 mm DV), along with the location of the

113 recording sites (green dots), from the tip (site #1) to the base (site #32). **b.** Firing intensity

114 maps displaying the RFs of the units recorded along the probe shown in **a**. The numbers

115 refer the sites each unit was recorded from. The reversal of the retinotopic progression (from

116 leftward to rightward) at sites #13-14 marks the boundary between areas LI and LL.

118 **Examples of tuning curves and spatiotemporal receptive fields in V1 and LL**

119 In both V1 and LL, neuronal responses to drifting gratings displayed a variety of tuning

120 profiles that matched well the RF structures inferred through STA. This is illustrated in Fig.

121 2, which reports, for each of two representative V1 (a-b) and LL (c-d) neurons: i) the tuning

122 curve as a function of the direction of the grating, when presented at the most effective SF

123 and TF; ii) the modulation of the firing rate elicited by the grating at the preferred direction;

124 and iii) the sequence of STA images showing the spatiotemporal evolution of the RF

125 structure. Each panel also reports the values of the metrics used to quantify the tuning

126 properties of the neurons (Methods). Orientation and direction tuning were measured using

127 the *orientation* and *direction selectivity indexes* (OSI and DSI), whose values range from 1

128 (maximal selectivity) to 0 (no selectivity), depending on the difference between the responses

129 to the preferred orientation/direction and the orthogonal/opposite one. We also computed a

130 *bimodal selectivity index* (BSI) to assess whether the tuning curve for orientation had

131 multiple peaks[27,28]. This index ranges from 0 (perfectly unimodal curve) to 1 (equal

responsiveness to two non-adjacent orientations), and can be taken as a measure of

complexity of tuning, with large BSI indicating tuning for multiple oriented features[27,28].

Finally, we computed a *modulation index* (MI) to quantify the extent to which the firing rate

of a neuron was entrained to the phase of the gratings[29,30], with MI > 3 indicating responses

that were strongly phase-locked to the stimulus temporal frequency. As for the

spatiotemporal filter estimated via STA, we used it as the linear stage of a Linear-Nonlinear

(LN) model of stimulus-response mapping[26] to predict the tuning curve of the neuron over the

direction axis and the time course of its response to the preferred grating (in both cases,

prediction accuracy was quantified as the fraction of response variance that was explained by

the model).

Fig. 2a shows an example V1 neuron with sharp orientation tuning, good direction

selectivity, and a response that was strongly modulated at the temporal frequency (4 Hz) of

the preferred grating. These properties match those of a *simple cell*[31], detecting the presence

of an oriented edge at a specific visual field location – hence the modulation of the firing rate,

produced by the phasic alternation of light and dark oriented stripes, while the preferred

grating swept across the neuron's RF. Such position-dependent neuronal firing suggests that

the response of the neuron to a visual pattern can be approximated as the sum of its responses

to the individual constituent elements (the "pixels") of the stimulus. Accordingly, the STA-

reconstructed RF (Fig. 2a.iii) had a Gabor-like, double-lobed appearance, with an orientation

matching the one corresponding to the peak of the tuning curve (Fig. 2a.i). When used as a

filter in a LN model, the STA-based RF accurately predicted the tuning of the neuron over

the direction and time axes (Fig. 2a.i and ii, respectively; black lines), thus confirming the

linearity of the stimulus-response relationship. By contrast, the example unit shown in Fig.

2b, while still being selective for a single orientation, displayed a highly non-linear behavior,

which is typical of the class of neurons known as *complex cells*[31]. This is shown by the lack

of modulation of the response to the preferred grating (Fig. 2b.ii), by the poorly defined

spatiotemporal structure of the STA-based RF (Fig. 2b.iii), and by the failure of the latter to

account for the tuning and time-modulation of the response (Fig. 2b.i-ii).

Fig. 2 Examples of neuronal tuning in V1 and LL. Representative V1 simple (**a**) and complex

(**b**) cells are shown in the upper panels (blue/black lines). Representative LL simple-like (**c**)

and complex-like (**d**) cells are shown in the lower panels (yellow/orange lines). In each

panel, subpanels i-iii illustrate different aspects of neuronal tuning. (i) The polar plot reports

the observed (light color) and predicted (dark color) tuning of the neuron for the direction of a

drifting grating, when shown at the preferred spatial (SF) and temporal (TF) frequencies of

the unit. Predictions were obtained using a linear-nonlinear (LN) model, derived from the

spike-triggered average (STA) images shown in iii. For ease of comparison, both the observed and predicted curves were normalized to their maximum. The plot also reports the fraction of variance of the tuning curve that was explained by the LN-model, as well as the values of several metrics that quantifies neuronal tuning: the orientation (OSI), direction (DSI) and bimodal (BSI) selectivity indexes. (ii) Raster plot (top) and peri-stimulus time histogram (PSTH; bottom; light color), showing the time course of the neuronal response to a drifting grating, when presented at the preferred SF, TF and direction. The bottom plot also reports the time course of the response, as predicted by the LN model (dark color), along with the fraction of variance explained by the model. For ease of comparison, both the observed and LN-predicted responses were normalized to their maximum. The top plot reports the value of the modulation index (MI), which measured to what extent the neuronal response was time-locked to the phase of the drifting grating. (iii) Spatial structure and time-evolution of the STA-estimated RF of the neuron. In every STA image, each pixel intensity value was independently z-scored, based on the null distribution of STA values obtained through a permutation test (Methods). As such, all RF intensity values are reported as distances (in units of standard deviation σ; gray scale bar in panel **d**.iii) from what expected in the case of no frame-related, linear information carried by the spikes.

Interestingly, simple-like and complex-like units were also found in area LL. For instance, Fig. 2c shows an LL neuron with a simple-like behavior, as indicated by the phase modulation of its response (Fig. 2c.ii; yellow dots and line), which was predicted with reasonable accuracy (orange line) by the STA-reconstructed RF. This is consistent with the well-defined spatiotemporal structure of the RF (Fig. 2c.iii), which, however, was not able to explain as much variance of the direction-tuning curve (Fig. 2c.i) as in the case of the example V1 simple cell (Fig. 2a.i). This could be due to the sensitivity of the neuron for multiple stimulus orientations, as shown by the large BSI value (0.52), which reflects the

presence of two peaks (at 0° and 240°) in the direction-tuning curve (Fig. 2c.i; yellow line) –

a behavior that cannot be captured by a RF with a linear, Gabor-like structure. Fig. 2d shows

instead an example LL unit that was sharply tuned for a single orientation, but displayed a

typical complex-like behavior: its response to the preferred grating was unmodulated (Fig.

2d.ii), and both the direction-tuning curve (Fig. 2d.i) and the response dynamics (Fig. 2d.ii)

were poorly explained by the STA-reconstructed RF (yellow vs. orange curves), which, in

turn, lacked any clear spatiotemporal structure (Fig. 2d.iii).

These examples illustrate how it is possible to compare the level of linearity of the

stimulus-response relationship for the neuronal populations recorded in V1 and LL, along

with the sharpens and complexity (e.g., bimodality) of their tuning for orientation. To guide

such comparison, we derived predictions about the evolution of neuronal tuning along an

object processing hierarchy, by assessing how our grating stimuli were represented in HMAX

– a neural network model of the ventral stream that is able to account for several qualitative

trends in the tuning properties of ventral neurons[23,27,32–35]. In its simplest implementation,

HMAX is a 4-layered, feed-forward network, with each layer consisting of either simple-like

(S) or complex-like (C) units (Fig. 3). The first layer (S1) is a bank of Gabor filters that

simulate V1 simple cells. In the second layer (C1), each unit performs a max pooling over a

set of S1 afferents with the same orientation tuning, but slightly different RF positions or

sizes. This yields orientation-tuned C1 units that are similar to V1 complex cells – i.e., they

have larger RFs (dashed circles in Fig. 3), with increased position- and size-tolerance, as

compared to their S1 afferents. In the third layer (S2), each unit performs a non-linear

template-matching computation over a set of C1 afferent units with different preferred

orientations. As a result, the S2 units are tuned for complex visual patterns, made of multiple

oriented features, like the neurons in higher-level stages of the primate ventral stream, such as

cortical area V4 and the inferotemporal cortex (IT). Finally, in the forth layer (C2), each unit

performs again a max pooling over S2 afferents that are tuned for the same visual pattern, but

with slightly different RF positions and sizes. This results in C2 units with complex shape

selectivity and large tolerance to position and size changes. Here, we used this basic 4-

layered architecture to predict how the build-up of shape tuning and invariance should affect

neuronal sensitivity to the orientation and temporal frequency of the gratings. In our

simulations, layers S1 and C1 correspond to the simple and complex cells of V1, while layers

S2 and, above all, C2, correspond to a downstream, higher-level area (such as LL).

Fig. 3 Sketch of the HMAX model implementation used in this study. The model is a

feedforward, 4-layered neural network that processes arbitrary input images through a

cascade of computations. The first layer (S1) consists of a bank of Gabor filters performing

local edge detection on small input image patches (dark gray circles), similar to V1 simple

cells. In the second layer (C2), each unit pools over many iso-oriented S1 units via a max-

like operation (dashed arrows), thus gaining some amount of position and scale tolerance,

similar to V1 complex cells (such expansion of the invariance field is represented by the light

gray rings). In the third layer (S2), each unit acquires tuning for more complex visual patterns

by combining the output of many C1 units with different orientation via a non-linear template-

matching operation (solid arrows). In the forth layer, each C2 unit applies again the max-

pooling operation to S2 units with the same shape tuning but different RF positions and

sizes, in order to further gain tolerance to such transformations. In our application, the input

images were drifting gratings, similar to those used in the neurophysiology experiment, so as

to obtain predictions about the evolution of the relevant tuning indexes (MI, OSI and BSI; see

Fig. 2) across consecutive stages of a ventral-like hierarchy.

The linearity of the stimulus-response relationship decreases from V1 to LL

To establish whether V1 and LL neurons differed in terms of the linearity of the stimulus-

response relationship, we first compared the extent to which neuronal responses in the two

areas were modulated by the temporal phase of the drifting gratings. Despite the presence of

both strongly phase-modulated and unmodulated units in both areas, the distributions of the

modulation index (MI) were strikingly different in V1 and LL (Fig. 4a). In agreement with

earlier studies of rat[36] and mouse[16,37] primary visual cortex, the MI distribution obtained in

V1 (blue curve) revealed to the existence of two roughly equi-populated classes of neurons,

falling, respectively, below and above the MI = 3 threshold that distinguishes complex-like

from simple-like cells. By contrast, in LL, most MI values were lower than 3, following a

distribution (orange curve) with a prominent peak at MI<1, which is indicative of a strong

prevalence of complex-like units. As a result, the median MI was much lower in LL than in

V1 (1.28 vs. 2.55; orange vs. blue line) and this difference was highly significant ($p < 0.001$;

Mann-Whitney U-test). Similarly, the fraction of simple-like cells in LL was half as large as

in V1 (Fig. 4b; $p<0.001$, χ^2 test).

As illustrated in Fig. 2d.ii, the poor sensitivity to the phase of the drifting gratings

observed in LL indicates that most neurons in this area respond to phasic stimuli with a

sustained firing. This suggests that, in LL, most neurons are tolerant to position changes of

their preferred visual stimuli. This interpretation is supported by the evolution of the

modulation index observed in HMAX (Fig. 4c), whose upper layer (C2), following the max-

pooling operation to gain translation invariance, contained units with much lower phase

sensitivity, as compared to the units of the previous layers. As a result, the MI distribution

obtained in C2 was remarkably similar to the one observed in LL.

Fig. 4 The entrainment of the neuronal response to the phase of drifting gratings decreases

from V1 to LL. **a.** Distributions of the modulation index (MI) for the populations of V1 (blue; *n*

= 105) and LL (orange; *n* = 104) neurons. Medians are shown as dashed lines (***p < 0.001;

one-tailed Mann-Whitney U-test). The gray-shaded area highlights the region of the MI axis

(MI > 3) corresponding to strongly phase-modulated units, i.e., simple-like cells. **b.** Fraction

of simple-like cells (i.e., units with MI > 3) in V1 (blue) and LL (orange; ***p < 0.001; χ^2 test).

c. Evolution of the MI distribution across the layers of the HMAX model (Fig. 3).

To further assess the linearity of the stimulus-response relationship in V1 and LL, we

evaluated the quality of the RFs inferred through the STA method. To this aim, each pixel

intensity value in a STA image was z-scored, based on the null distribution of STA values

obtained for that pixel, after randomly permuting the association between frames of the

movie and spike times 50 times. This allowed expressing the intensity values of the STA

image in terms of their difference (in units of standard deviation) from what expected in the

case of no frame-related information carried by the spikes. We then computed a *contrast*

index (CI; Methods and Supplementary Fig. 1) to measure the amount of signal contained in

the image and establish a conservative threshold (CI > 5.5), beyond which the linear RF

structure of a neuron could be considered as well defined.

Fig. 5a shows the 10 best STA-based RFs in each area, sorted according to the

magnitude of their CI, from largest to smallest. In V1, most of these RFs featured equally

prominent excitatory and inhibitory regions, often displaying a sharp, Gabor-like structure,

while in LL the best STA images typically presented a single lobe, with much lower contrast.

As a result, the median CI was higher for V1 than for LL neurons (blue vs. orange dashed

line in Fig. 5b; *p* < 0.001; one-tailed Mann-Whitney U-test), and the fraction of units with

well-defined linear RFs (i.e., with CI > 5.5) was 5 times larger in V1 than in LL (Fig. 5c; *p* <

0.001, χ^2 test). We also observed a stark difference between the two areas in terms of the

number of lobes contained in a STA image. To count the lobes, we binarized each image, by

applying a threshold to the modulus of its intensity values (Methods and Supplementary Fig.

1; this analysis was restricted to the units with well-defined linear RFs). Regardless of the

choice of the binarization threshold, the distribution of lobe counts peaked at 1 in both areas,

but had a heavier tail in V1 than in LL (compare matching rows in Fig. 5d), resulting, in most

cases, in a statistically significant difference between the two areas (Fisher's exact test; * $p <$

0.05; ** $p < 0.01$). Overall, this indicates that, in many cases, the responses of V1 neurons

could be well approximated as a linear, weighted sum of the luminance intensity values

falling inside their RFs – hence the sharp, multi-lobed STA images. By comparison, the

lower-contrast, structurally simpler RFs yielded by STA in LL suggest a dominant role of

non-linear computations in establishing the stimulus-response relationship in this area. In

fact, in the case of prevalently non-linear units, the STA method would be able to reconstruct

at most their linear sub-parts[38–40] – a sort of linear "residue" of the actual non-linear filter.

Such linear residue would still show, in some cases, the position and main orientation of the

underlying filter, but would fail short at accounting for the full richness and complexity of its

structure. This conclusion was supported by the tendency of the STA-based RFs to explain a

lower fraction of variance of the orientation tuning curves in LL, as compared to V1

(Supplementary Fig. 2). Taken together with the prevalence of complex-like units in LL (Fig.

4), these findings are consistent with the non-linear computations that are expected to build

invariance along an object-processing hierarchy.

Fig. 5 Spike-triggered average yields better-defined and structurally richer receptive fields in

V1 than in LL. **a.** Spatial structure of the ten best linear RFs obtained in V1 (top row) and LL

(bottom row) using the STA method. The quality of each RF was assessed by computing a

contrast index (CI) that measured the amount of signal contained in a STA image

(Supplementary Fig. 1a and c and Methods). For each neuron, the RF shown here is taken

at the time before the spike when CI was maximum (the corresponding CI value is reported

above each STA image). As explained in Fig. 2, each pixel intensity value in a STA image

was independently z-scored according to the null distribution yielded by a permutation test;

the resulting z-scored values are reported here in units of standard deviation σ (gray scale

bar). **b.** CI distributions for the populations of V1 (blue; *n* = 105) and LL (orange; *n* = 104)

neurons. Medians are shown as dashed lines (***p < 0.001; one-tailed Mann-Whitney U-

test). The gray-shaded area highlights the region of the CI axis (CI > 5.5) corresponding to

units with well-defined linear RFs. **c.** Fraction of units with well-defined linear RFs (i.e., with

CI > 5.5) in V1 (blue) and LL (orange; ***p < 0.001; χ^2 test). **d.** Heat maps showing the

distributions of lobe counts (abscissa) for the units with well-defined linear RFs (i.e., with CI

330   > 5.5) in V1 (blue; *n* = 13) and LL (red; *n* = 56) as a function of the binarization threshold

331   (ordinate) used by the lobe-counting algorithm (Supplementary Fig. 1b and d and Methods).

332   Stars indicate threshold values for which the two distributions were significantly different (*p

333   < 0.05, **p < 0.01; Fisher exact test).

Sharpness and complexity of orientation tuning follow opposite trends from V1 to LL

Next, we compared the V1 and LL neuronal populations in terms of the shape and sharpness

of the orientation tuning curves obtained in the two areas. As shown in Fig. 6a, in area LL

most units had OSI lower than 0.5 (orange curve), with a median of 0.41 (orange line), while

in V1 the peak of the OSI distribution was in the 0.6-0.8 range, with a median of 0.53. The

difference between the two OSI distributions was highly significant ($p < 0.01$; Kolmogorov-

Smirnov test), as it was the difference between their medians ($p < 0.001$; one-tailed, Mann-

Whitney U-test). Following a convention established in previous studies (Supplementary

Table 2) we classified as orientation-selective the units with OSI > 0.6, and we compared the

fraction of units above such threshold in the two areas (Fig. 6b). In V1, the proportion of

selective cells was twice as large as in LL (40% vs. 18%), and such difference was, again,

highly significant ($p < 0.001$; χ^2 test).

To check the consistency of this finding with ventral-like processing, we looked at the

evolution of orientation tuning in HMAX. As shown in Fig. 6c, in the model, the OSI

distribution underwent an abrupt shift towards much lower values in the transition from the

C1 layer, corresponding to V1 complex cells, to the S2 layer, corresponding to a downstream

area, where tuning for combinations of multiple oriented elements is achieved using a non-

linear template matching operation (see Fig. 3). The shape of the OSI distribution was then

maintained in the C2 layer, performing the max-pooling operation over the S2 afferents. This

trend shows that, in HMAX, building tuning for complex visual patterns leads to a strong

reduction of orientation tuning. As such, the drop of orientation selectivity observed from V1

to LL can be taken as indication that LL neurons are tuned to more complex combinations of

visual features, as compared to V1 units.

Fig. 6 Orientation selectivity decreases from V1 to LL. **a.** Distributions of the orientation

selectivity index (OSI) for the populations of V1 (blue; $n = 105$) and LL (orange; $n = 104$)

neurons. Medians are shown as dashed lines (**$p < 0.01$; one-tailed Mann-Whitney U-test).

The gray-shaded area highlights the region of the OSI axis (OSI > 0.6) corresponding to

orientation-selective units. **b.** Fraction of orientation-selective cells (i.e., units with OSI > 0.6)

in V1 (blue) and LL (orange; ***$p < 0.001$; χ^2 test). **c.** Evolution of the OSI distribution across

the layers of the HMAX model (Fig. 3).

Support to this conclusion came from comparing the two areas in terms of the

tendency of the orientation tuning curves to be bimodal (Fig. 7a). In V1, most units had BSI

equal or close to zero (i.e., virtually perfect unimodal tuning), with the distribution dropping

sharply at larger BSI values (blue curve). In LL, the BSI distribution also peaked at zero, but

featured a heavier tail, with a secondary peak above 0.5 (orange curve). As a result, the two

distributions and their medians were significantly different ($p < 0.05$; Kolmogorov-Smirnov

and one-tailed, Mann-Whitney U-test, respectively) and the fraction of neurons with bimodal

tuning (i.e., with BSI > 0.5) was more than twice as large in LL than in V1 ($p < 0.05$, χ^2 test;

Fig. 7b). Once again, a similar trend was observed in HMAX (Fig. 7c), where the BSI

distribution displayed a heavier tail in the deeper layers (S2 and C2) than in the early ones

(S1 and C1). This supports the interpretation that the decrease of OSI from V1 to LL, along

with the concomitant increase of BSI, results from an increment of the complexity of tuning

of LL neurons – a property that is consistent with their involvement in ventral processing. By

contrast, no significant differences were found in terms of direction selectivity

(Supplementary Fig. 3), which suggests a lack of specialization of LL for motion processing,

as compared to V1.

Fig. 7 The tendency to be tuned for multiple orientations increases from V1 to LL. **a.**

Distributions of the bimodal selectivity index (BSI) for the populations of V1 (blue; n = 105)

and LL (orange; n = 104) neurons. Medians are shown as dashed lines (*p < 0.05; one-tailed

Mann-Whitney U-test). The gray-shaded area highlights the region of the BSI axis (BSI >

0.5) corresponding to units with bimodal tuning. **b.** Fraction of cells with bimodal tuning (i.e.,

with BSI > 0.5) in V1 (blue) and LL (orange; *p < 0.05; χ^2 test). **c.** Evolution of the BSI

distribution across the layers of the HMAX model (Fig. 3).

Discussion

In this study, we investigated whether LL (the most temporal among rat lateral extrastriate

areas) displays tuning properties that are consistent with its involvement in ventral-like

processing of shape information. Previous anatomical and lesion work has causally

implicated rat lateral areas in object recognition[41,42], but only a handful of studies have

probed visual processing in these regions at the functional level[24,25,43,44]. Two of them, in

particular, have explicitly tested the aptness of LL at supporting transformation-tolerant

recognition of visual objects[24,25] – the hallmark property of the ventral pathway[21]. In both

cases, linear classifiers were applied to test the ability of LL neurons to support invariant

decoding of object identity, but only Tafazoli and colleagues[24] found LL to be superior to V1

in such a task. As explained in the Introduction, the conflicting findings of these previous rat

studies, as well as the limited functional understanding of ventral processing in mouse visual

cortex[3,6,8], motivated our search for further evidence of ventral computations in LL.

To be fully complementary with our previous study of rat ventral areas[24], we did not

probe LL representations using visual objects. With the goal of devising a more intuitive and

standardized approach to the study of ventral processing in rodents, we deployed instead

drifting oriented gratings, and we compared the V1 and LL neuronal populations in terms of:

1) the phase-sensitivity of their responses; 2) the goodness of the RF structures recovered

through STA; and 3) the sharpness and complexity (i.e., bimodality) of their tuning for

orientation. Obviously, this approach requires obtaining clear predictions about how these

properties should evolve along a ventral-like pathway. In our study, we achieved such

predictions based on the simulations of a computational model of the ventral stream (HMAX)

and a careful survey of the monkey literature.

HMAX is a feedforward neural network that was originally developed to explain the

emergence of selective, yet transformation-tolerant representations of visual objects along the

primate ventral stream[23]. Over the years, the model has provided useful computational

insights about shape tuning in V4 and IT[23,27,32–35], and human perception of visual objects[35,45].

The model shares the same basic architecture of more recent artificial vision systems (e.g.,

deep convolutional neural networks[46]), with alternating layers of selectivity-increasing and

tolerance-increasing pooling, but it is computationally simpler, since, in its basic

instantiation, it has only 4 layers and does not involve any supervised learning of feature

representations. While this can easily explain why HMAX has been surpassed by deep-

learning networks as a state of the art machine vision system[47,48], its simpler and static

structure makes it an ideal conceptual model to isolate the role of the selectivity- and

invariance-building operations in establishing the tuning properties of ventral neurons. As

shown by our simulations, HMAX makes very specific predictions about how the tuning for

oriented gratings should evolve from V1 to downstream ventral areas. Because of the

tolerance-building operation (the max-pooling), phase-sensitivity should decrease (Fig. 4c).

At the same time, because of the selectivity-building computation (the template-matching

pooling), orientation tuning should become smaller (Fig. 6c), while neurons acquire

preference for multiple orientations (Fig. 7c). Critically, all these trends were matched by the

empirical evidence gathered in our study, when comparing V1 to LL (Figs. 4a-b, 6a-b and 7a-

b), thus suggesting a specialization of the latter for ventral-like processing.

To check if this conclusion was also supported by a comparison with the monkey

literature, we performed a simple meta-analysis of the trends of variation of orientation

tuning and phase-sensitivity to drifting gratings across areas V1, V4 and IT of the ventral

stream. In V1, the fraction of simple cells reported by various authors is quite variable,

ranging from ~16% to 63% (Supplementary Table 1), with a mean across studies of ~41%

(blue bar in Fig. 8a). According to the few studies that investigated the phase-dependence of

neuronal responses to grating stimuli in downstream areas (Supplementary Table 1), the

proportion of simple-like cells diminishes to ~14% in V4, to become zero in IT (yellow and

orange bars in Fig. 8a), resulting in an overall significant decrement along the ventral stream

($p < 0.01$, $F_{2,13} = 7.25$, one-way ANOVA). With regard to orientation selectivity, most

authors report a very large fraction of orientation-tuned cells in monkey V1 (Supplementary

Table 2), with a mean across studies close to 89% (blue bar in Fig. 8B). This proportion

significantly decreases along downstream areas ($p < 0.001$, $F_{2,14} = 46.17$, one-way ANOVA),

with ~65% and ~19% of orientation-tuned neurons reported, respectively, in V4 and IT

(yellow and orange bars in Fig. 8b; see also Supplementary Table 2). These trends are

confirmed by the few studies that applied the same experimental design to directly compare

orientation tuning in V1 and either V4[28] or IT[49,50]. Vogels and Orban[49,50] found ~85% of

orientation-tuned neurons in V1, compared to just ~14% in IT. David and colleagues[28]

reported a similar figure for V1, while in V4 they found that only 50% of neurons were

orientation-tuned. In addition, they found that the fraction of cells with bimodal tuning was

more than twice as large in V4 (~28%) than in V1 (~11%), in agreement with the increasing

proportion of neurons that, in V4, are tuned for the combinations of oriented elements found

in corners and curved boundaries[51–54].

Fig. 8 Meta-analysis of the trends of variation of phase sensitivity and orientation tuning to drifting gratings across the primate ventral stream. **a.** Fraction of cells that have been reported as being strongly modulated by the phase of drifting gratings (i.e., simple-like cells) in areas V1 (red; n = 10), V4 (yellow; n = 3) and IT (red; n = 1) of the monkey ventral stream (mean across n studies in each area ± SE; see Supplementary Table 1). The drop of phase modulation across the three areas was statistically significant (p < 0.01, one-way ANOVA). **b.** Fraction of cells that have been classified as being tuned to the orientation of drifting gratings in areas V1 (red; n = 7), V4 (yellow; n = 4) and IT (red; n = 4) of the monkey ventral stream (mean across n studies in each area ± SE; see Supplementary Table 2). The drop of orientation tuning across the three areas was statistically significant (p < 0.001, one-way ANOVA).

Among rodent studies of visual extrastriate areas, our results are the first that are in complete agreement with the monkey literature reviewed above and are fully consistent with the computational principles thought to be at the root of ventral processing (as implemented in the HMAX simulations). In mice, area LL has not been identified, but areas LM (lateromedial) and LI (laterointermediate), which, as in rats, are located progressively more

lateral to V1 (see Fig. 1a), have been attributed to the ventral stream based on anatomical

considerations[55,56] and have been tested with drifting gratings in several electrophysiological

and imaging studies, often along with other medial and parietal visual areas[13,14,16,17,57].

Consistently with our findings (Fig. 4), the only study that measured the phase dependence of

neuronal responses in V1 and lateral visual areas of the mouse found that the latter had a

lower proportion of simple cells (15% vs. 38% in V1)[16]. Conversely, the authors reported no

difference between the areas in terms of OSI. This result contrasts with the general increase

of orientation tuning that was found in nearly all extrastriate areas (compared to V1) by

Marshell and colleagues[14], although the increment of OSI was much larger in putative dorsal-

stream areas than in LM and LI. A significant increase of OSI in LM, relative to V1, was also

observed by Tohmi and colleagues[18], while other authors found no differences between V1

and some of the putative dorsal-stream areas in terms of orientation tuning[13,17]. As for rat

cortex, Vermaercke and colleagues[25] found the opposite trend of that observed in our study –

i.e., a progressive increase of OSI from V1 to LL and beyond[25].

Different causes can be at the root of such discrepancies among rodent studies. In

mice, many experiments were based on calcium imaging, performed using different

indicators (e.g., OGB-1[14] vs. GCaMP3[13]), which diverge from a perfectly linear relationship

between fluorescence changes and underlying spiking activity in an-indicator specific way[58].

As pointed out by Niell[3], this could potentially distort the orientation tuning curves and bias

the OSI measurements, as compared to approaches where well-isolated single-units are

recorded with micro-electrodes, as in our study. Other important differences could concern

the specific stimuli that were used by different authors. For instance, while we presented very

large (60º×110º), full-field gratings, Vermaercke and colleagues[25] used smaller (33º) circular

gratings, shown at the center of each recorded receptive field. Our presentation protocol

assured that, for most neurons in both areas, the stimuli covered the entire *classical* receptive

field and, very likely, a large fraction of the *extra-classical* receptive field, where surround-

suppression contributes to shape tuning both in monkey[1,2] and rodent[59–63] visual cortex. By

contrast, the smaller and more localized gratings used in [25] likely covered an increasingly

smaller fraction of both the classical and extra-classical receptive fields along the V1-LM-LI-

LL progression, given that RF size gradually increases along rat lateral extrastriate areas,

being twice as large in LL as in V1[24]. This, in turn, may have prevented the tuning for

multiple oriented elements, located at different RF locations, to emerge in neurons with larger

RFs, thus artificially boosting OSI in higher-order areas. Finally, another factor that is worth

considering is whether neuronal recordings were performed in anesthetized or awake animals.

In general, both volatile (e.g. isofluorane) and injectable (e.g., urethane and ketamine)

anesthetics can depress cortical activity in high-order areas[64], put the cortex in a highly

synchronized state[65], and alter the excitation-inhibition balance that is typical of the wakeful

state[59,66]. However, most of these shortcomings can be prevented by applying anesthesia

protocols that, as the one used in our study, are based on a combination of dissociative

analgesics (such as fentanyl) with α2 receptor agonists (such as medetomidine or xylazine).

This form of anesthesia maximizes retinal function[67], allows for desynchronized cortical

states, and results in stimulus-driven responses that are similar to those of the wakeful

state[68,69]. In addition, the authors that compared neuronal activity in mouse visual cortex

under anesthesia and during active wakefulness found that several key tuning properties, both

in V1 and extrastriate areas, were very similar in the two conditions [37,70–73]. As such, it is very

unlikely that the choice of using or not anesthesia determined the differences found in the

rodent literature, with regard to orientation selectivity and other tuning properties.

Ultimately, four considerations support the strength and reliability of our conclusions,

as compared to previous studies of rodent visual cortex based on gratings. First, the full

agreement with the trends found across the monkey ventral stream. Second, the full

agreement with the predictions derived by simulating the basic computational architecture of

the ventral stream. Third, the self-consistency of our findings – for instance, the reduction of

orientation tuning from V1 to LL was matched by a concomitant increase of bimodal tuning,

with both trends pointing to the development of selectivity for complex visual patterns in LL.

Forth, the agreement with our previous investigation of rat lateral visual areas, where we

found the signature of specialized processing of visual objects, and the consistency with the

advanced processing of shape information reported, for rats, by several behavioral studies[74–

76]. In the light of these arguments, we believe that our study provides strong evidence of the

specialization of LL for ventral-like computations, thus adding crucial support to a still

unsettled and debated question. At the methodological level, our study offers a standardized

and easily interpretable way to carry out a large-scale screening of ventral processing across

rodent visual cortical areas. This could help optical imaging studies finding the yet missing

functional signature of ventral processing in mouse visual cortex (e.g., by analyzing existing

large datasets of stimulus-response associations, as the one made available by the Allen Brain

Observatory[77]). In this regard, having provided clear predictions about the trends of variations

of several neuronal tuning properties, based on computational modeling and an exhaustive

survey of the monkey literature, will likely serve as a reference to guide future explorations

of ventral functions in both mice ad rats.

Methods

Animal preparation and surgery. All animal procedures were in agreement with

international and institutional standards for the care and use of animals in research and were

approved by the Italian Ministry of Health: project N. DGSAF 22791-A, submitted on Sep. 7,

2015 and approved on Dec. 10, 2015 (approval N. 1254/ 2015-PR). 18 naïve Long-Evans

male rats (Charles River Laboratories), with age 3-12 months and weight 300-700 grams,

underwent extracellular recordings in either primary visual cortex (V1) or laterolateral (LL)

extrastriate visual cortex. Each rat was anesthetized with an intraperitoneal (IP) injection of a

solution of 0.3 mg/kg of fentanyl (Fentanest®, Pfizer) and 0.3 mg/kg of medetomidin

(Domitor®, Orion Pharma). The level of anesthesia was monitored by checking the absence

of tail, ear and hind paw reflex, as well as monitoring blood oxygenation, heart and

respiratory rate through a pulse oximeter (Pulsesense-VET, Nonin). A constant flow of

oxygen was delivered to the rat throughout the experiment to prevent hypoxia. A constant

level of anesthesia was maintained through continuous IP infusion of the same anesthetic

solution used for induction, but at a lower concentration (0.1 mg/kg/h Fentanyl and 0.1 g/kg/h

Medetomidin), by means of a syringe pump (NE-500; New Era Pump Systems). Temperature

was thermostatically kept at 37°C using a heating pad to prevent anesthesia-induced

hypothermia.

After induction, the rat was secured to a stereotaxic apparatus (Narishige, SR-5R)

and, following a scalp incision, a craniotomy was performed over the target area in the left

hemisphere (typically, a 2x2 mm^2 window) and the dura was removed to allow the insertion

of the electrode array. When targeting V1, the coordinates of penetration were ~6.5 mm

posterior from bregma and ~4.5 mm left to the sagittal suture (i.e., AP 6.5, ML 4.5). When

targeting LL, the coordinates were ~1 mm anterior from lambda and ~1 mm medial from the

cranial ridge (i.e., AP 8, ML 5). Throughout the procedure, the rat eyes were protected from

direct light and kept hydrated by repeated application of an ophthalmic ointment (Epigel®,

Ceva Vetem).

Once the surgical procedure was completed, and prior to probe insertion, the stereotax

was placed on a rotating platform and the rat's left eye was covered with black, opaque tape,

while the right eye (placed at 30 cm distance from the monitor) was immobilized using a

metal eye-ring anchored to the stereotax. The platform was then rotated, so as to align the

right eye with the center of the stimulus display and bring the binocular portion of its visual

field to cover the left side of the display. During the recordings, the eye and cortex were

periodically irrigated using saline solution to keep them properly hydrated.

Neuronal recordings. Extracellular recordings were performed using single-shank 32-

channel silicon probes (NeuroNexus Technologies) with site recording area of 775 μm^2 and

25 μm of inter-site spacing. After grounding (by wiring the probe to the animal's head skin),

the electrode was manually lowered into the cortical tissue using an oil hydraulic

micromanipulator (Narishige, MO-10; typical insertion speed: ~ 5 μm/s), up to the chosen

insertion depth (~800-1,000 μm from the cortical surface when targeting V1, and ~2,500 μm

when targeting LL). To reach LL, the probe was tilted of 30° relative to the cortical surface

(Fig. 1a), whereas it was inserted perpendicularly into V1. Extracellular signals were

acquired using a system three workstation (Tucker-Davis Technologies) with a sampling rate

of 25 kHz. Before insertion, the probe was coated with Vybrant® DiI cell-labeling solution

(Invitrogen, Oregon, USA), to allow visualizing the probe insertion track *post-mortem*,

through histological procedures. To this aim, at the end of the recording session, an

electrolytic lesion was also performed by delivering current (5 μA for 2 seconds) through the

4 deepest channels at the tip of the shank.

Visual stimuli. During a recording session, two kinds of visual stimulation protocols were

administered to the rat.

A 15 min-long receptive field (RF) mapping procedure was used to precisely identify

the visual area each neuron was recorded from (see details below) and optimize the location

of the RFs for the main presentation protocol (i.e., ensure that most RFs fell inside the

monitor, by rotating the platform or repositioning the eye through adjustments of the eye-

ring). During the RF mapping protocol, the animal was presented with 10°-long drifting bars

with four different orientations (0°, 45°, 90° and 135°), tiling a grid of 66 different visual field

locations (i.e., 6 rows, spanning vertically 50°, and 11 columns, spanning horizontally 100°).

The bars were white over a black background. During presentation of these stimuli, multiunit

spiking responses (MUA) were plotted as a function of screen position in real-time, so as to

estimate the positions of the RF centers across the recording sites of the probe. This allowed

identifying in real-time when area LL was reached during an oblique probe insertion.

Specifically, area LL was identified by the third "rightwards" (i.e., from nasal to temporal)

reversal of the retinotopy at a recording depth close to 2.5 mm DV[24] (Fig. 1). The same

analysis was applied off-line to the well-isolated single units obtained by spike sorting (see

below) to precisely identify the neurons that were recorded from LL.

Once the probe was positioned in the final recording location, the main presentation

protocol was administered. The rat was presented with: 1) 1s-long drifting gratings, made of

all possible combinations of 3 spatial frequencies (SF; 0.02, 0.04 and 0.08 cpd), 3 temporal

frequencies (TF; 2, 4 and 8 Hz), and 12 directions (from 0° to 330°, in 30° increments); and

2) 30s-long movies of spatially and temporally correlated noise. To allow for a precise

estimate of neuronal tuning properties, each grating stimulus was presented in 20 repeated

trials, while 80 distinct noise movies were shown for an overall duration of 40 minutes. All

stimulus conditions were randomly interleaved, with a 1s-long inter stimulus interval (ISI),

during which the display was set to a uniform, middle-gray luminance level (later used to

estimate spontaneous firing rates; see below). To generate the movies, random white noise

movies were spatially correlated by convolving them with a Gaussian kernel. The kernel full

width at half maximum (FWHM) was chosen to match a 0.02 cpd SF, which was found to

elicit a robust spiking response in a series of pilot experiments. For the same reason (i.e., to

increase the chance of evoking spikes), temporal correlations were also introduced, by

convolving the movies with a causal exponential kernel with a 33 ms decay time-constant.

Stimuli were generated and controlled in MATLAB (The MathWorks) using the

Psychophysics Toolbox package and displayed with gamma correction on a 47-inch LCD

monitor (SHARP PNE471R) with 1920x1080 pixel resolution, 220 cd/m^2 maximum

brightness and spanning a visual angle of 110° azimuth and 60° elevation. Grating stimuli

were presented at 60 Hz refresh rate, whereas noise movies were played at 30 Hz.

Histology. At the end of the recording session, each animal was deeply anesthetized with an

overdose of urethane (1.5 gr/kg) and perfused transcardially with phosphate buffer saline

(PBS) 0.1 M, followed by 4% paraformaldehyde (PFA) in PBS 0.1 M, pH 7.4. The brain was

then removed from the skull, post-fixed in 4% PFA for 24 h at 4°C, and then immersed in

cryoprotectant solution (15% w/v sucrose in PBS 0.1 M, then 30% w/v sucrose in PBS 0.1

M) for 48 h at 4 °C. The brain was finally sectioned into 30μm-thick coronal slices using a

freezing microtome (Leica SM2000R, Nussloch, Germany). Sections were mounted

immediately on Superfrost Plus slides and let dry at room temperature overnight. A brief

wash in distilled water was performed, to remove the excess of crystal salt sedimented on the

slices, before inspecting them at the microscope. Each slice was then photographed with a

digital camera adapted to a Leica microscope (Leica DM6000B-CTR6000, Nussloch,

Germany), acquiring both a DiI fluorescence image (700 nm DiI filter) and a bright-field

image at 2.5X and 10X magnification. Following the acquisition of this set of images, the

sections displaying the electrode fluorescent track were further stained for Nissl substance

using a Cresyl Violet Acetate solution, and new pictures were taken at 2.5X and 10X

magnification. By superimposing the fluorescence, bright-field and Nissl-stained images, it

was possible to reconstruct the tilt and the anteroposterior (AP) position of the probe during

the recording session.

Selection of the single units included in the analyses. Responses of single units were

isolated offline by applying the spike sorting package KlustaKwik-Phy[78]. Automated spike

detection, feature extraction and expectation maximization (EM) clustering were followed by

manual refinement of the sorting using a customized version of the "Kwik-GUI" interface.

Specifically, the manual curation of the automatic output was performed by taking into

consideration many features of the candidate clusters: 1) the distance between their centroids

and their compactness in the space of the principal components of the waveforms (a key

measure of goodness of spike isolation); 2) the shape of the auto- and cross-correlograms

(important to decide whether to merge or not two clusters); 3) the variation, over time, of the

principal component coefficients of the waveform (important to detect and take into account

the effects of possible electrode drifts); and 4) the shape of the average waveform (to exclude,

as artifacts, clearly non-physiological signals). Clusters suspected to contain a mixture of one

or more single units were separated using the "reclustering" feature of the GUI (i.e., by

rerunning the EM clustering algorithm on the spikes of these clusters only). At the end of the

manual refinement step, only responsive, well-isolated single units, with reproducible firing

across repeated stimulus presentations, were included in the dataset used to perform all

subsequent analyses. Specifically, such units were defined by having: i) less than 0.5% of

"rogue" spikes within 2 ms in their autocorrelogram (i.e., units displaying a clear refractory

period); ii) a mean stimulus response firing rate of 2 spikes/s above baseline (i.e., responsive

units); and iii) responsiveness in at least 30% of the trials in one or more stimulus conditions

(i.e., stable isolation during the recording and reproducible stimulus-evoked response). We

also applied an additional, very loose screening on the reproducibility of the firing rate across

repeated stimulus presentations, by including only neurons with a mean correlation

coefficient of the direction-tuning curve across trials not lower than 0.03. The average

baseline (spontaneous) firing-rate of each well-isolated unit was computed by averaging its

spiking activity over every ISI condition. These criteria led to the selection of 105 units in V1

and 104 units in LL.

Analysis of the responses to drifting gratings. The response of a neuron to a drifting

grating was computed by counting how many spikes the neuron fired (on average, across

repeated presentations of the stimulus) during the whole duration of stimulus presentation,

and then subtracting the spontaneous firing rate (see above). To quantify the tuning of a

neuron for the orientation and direction of drifting gratings, we computed two standard

metrics, the orientation and direction selectivity indexes (OSI and DSI), which are defined as:

$\mathrm{OSI} = (R_{\mathrm{pref}} - R_{\mathrm{ortho}})/(R_{\mathrm{pref}} + R_{\mathrm{ortho}})$, and $\mathrm{DSI} = (R_{\mathrm{pref}} - R_{\mathrm{opposite}})/(R_{\mathrm{pref}} + R_{\mathrm{opposite}})$,

where R_{pref} is the response of the neuron to the preferred direction, R_{ortho} is the response to

the orthogonal direction, relative to the preferred one (i.e., $R_{\mathrm{ortho}} = R_{\mathrm{pref}} + \pi/2$), and

R_{opposite} is the response to the opposite direction, relative to the preferred one (i.e.,

$R_{\mathrm{opposite}} = R_{\mathrm{pref}} + \pi$). Values close to one indicate very sharp tuning, whereas values close

to zero are typical of untuned units.

The modulation of the spiking response to drifting gratings at the temporal frequency

f_1 of the stimulus was quantified by a modulation index (MI) adapted from [29] and defined as:

$$\mathrm{MI} = \left| \frac{PS(f_1) - \langle PS \rangle_f}{\sqrt{\langle PS^2 \rangle_f - \langle PS \rangle_f^2}} \right|,$$

where PS indicates the power spectral density of the stimulus-evoked response, i.e., of the

peri-stimulus time histogram (PSTH), and $\langle\ \rangle_f$ denotes the average over frequencies. This

metric measures the difference between the power of the response at the stimulus frequency

and the average value of the power spectrum in units of its standard deviation. The power

spectrum was computed by applying the Blackman-Tukey estimation method to the baseline-

subtracted, 10ms-binned PSTH. Being MI a standardized measure, values greater than 3 can

be interpreted as signaling a strong modulation of the firing rate at the stimulus frequency

(typical of simple-like cells), whereas values smaller than 3 indicate poor modulation (typical

of complex-like cells).

Bimodal tuning (i.e., the presence of two distinct peaks in the orientation-tuning

curve) was quantified by the Bimodal Selectivity Index[27,28], defined as

$\text{BSI} = \left(R_{\text{2nd peak}} - R_{\text{2nd trough}}\right) / \left(R_{\text{1st peak}} - R_{\text{1st trough}}\right)$, where $R_{\text{1st peak}}$ and $R_{\text{2nd peak}}$ indicate

the two largest peaks in the orientation-tuning curve (with $R_{\text{1st peak}} > R_{\text{2nd peak}}$), and

$R_{\text{1st trough}}$ and $R_{\text{2nd trough}}$ indicate the deepest troughs (with $R_{\text{1st trough}} < R_{\text{2nd trough}}$). This

index takes values close to one for tuning curves displaying two equally high peaks and close

to 0 for tuning curves with a single peak.

Analysis of the responses to the noise movies. We used the spike-triggered average (STA)

analysis[26] to estimate the linear RF structure of each recorded neuron. The method was

applied to the spike trains fired by the neuron in response to the spatiotemporally correlated

noise (see above). The method yields an ordered sequence of images, each showing the linear

approximation of the spatial RF at different times before spike generation (see examples in

Fig. 2). To take into account the correlation structure of our stimulus ensemble and prevent

artifactual blurring of the reconstructed filters, we "decorrelated" the resulting STA images

by dividing them by the covariance matrix of the whole stimulus ensemble[26], using Tikhonov

regularization to handle covariance matrix inversion. Statistical significance of the STA

images was then assessed pixelwise via a permutation test. After randomly reshuffling the

spike times, the STA analysis was repeated multiple times (n=50) to derive a null distribution

of intensity values for the case of no linear stimulus-spike relationship. This allowed z-

scoring the actual STA intensity values using the mean and standard deviation of this null

distribution (Fig. 2 and 5). The temporal span of the spatiotemporal linear kernel

reconstructed via STA extended till to 330 ms before spike generation, corresponding to a

duration of 10 frames of the noise movie played at 30 Hz (Fig. 2).

After estimating the linear spatiotemporal structure of a RF with STA, we used it as a

filter in the input stage of a classical Linear-Nonlinear (LN) model of stimulus-response

relationship[26]. To obtain a prediction of the tuning of the neuron over the direction axis, the

sequence of frames of each drifting grating was fed as an input to the STA-estimated linear

filter. The output of the filter was then passed through a rectifying nonlinearity with unit gain

to obtain the final response of the model to each stimulus frame. We finally integrated the

response of the LN model through time to predict the activity of the neuron for each direction

of the tuning curve. The agreement between the LN-predicted and observed tuning curves

was quantified by computing the fraction of explained variance (dark vs. light tuning curves

in Fig. 2.i). In addition, we also quantified how well the time course of the neuronal response

to the preferred grating was explained by the time course of the LN-model prediction (dark

vs. light dynamics in Fig. 2.ii), again, in terms of explained variance.

We also estimated the amount of signal contained in a given STA image by defining a

quality metric based on a measure of maximal local contrast. Specifically, we used MATLAB

"rangefilt" function (MATLAB Image Processing toolbox) to compute the local contrast in a

STA image over convolutional patches with size equal to one fifth of the total image size and

stride 1 (the local contrast in every patch was measured as the difference between the

maximum and the minimum image intensity values within the patch itself). From the

resulting local-contrast map (Supplementary Fig. 1a and c, middle plot), we obtained a

distribution of contrast intensity values (Supplementary Fig. 1a and c, rightmost plot), and we

defined a contrast index (CI) by taking the 0.9 quantile of this distribution (dashed line; the

0.9 quantile was chosen, instead of simply using the maximum local-contrast value, to make

this measure more noise-robust). This CI metric was then used to quantify the amount of

signal contained in the STA image. A STA-based RF was considered as well defined if,

among the sequence of STA images corresponding to each pre-spike-generation time lag (see

examples in Fig. 2), the one with the highest contrast had CI > 5.5 (usually, such highest-

contrast image was the third in the sequence, corresponding to 66-99 ms before the spiking

event; see examples in Fig. 5a). It should be noted that, since the intensity values of the

original STA images (Supplementary Fig. 1a and c, leftmost plot) were expressed as z-scores

(see above), the 5.5 threshold can be interpreted in terms of peak-to-peak (i.e. white-to-black)

distance in sigma units of the z-scored STA values.

To further analyze the spatial structure of each well-defined, STA-based RF we

automatically counted how many distinct lobes the highest-contrast STA image obtained for a

unit contained. To this aim, the selected image was background-suppressed to enhance the

high-intensity regions within the RF and reduce noise-driven false lobe detections. We then

took the modulus of the resulting image and we set a threshold over its z-score values

(ranging from 3 to 6 units of standard deviations; Supplementary Fig. 1b and d). Based on

such binarized image, we computed: i) the centroid position of each simply connected region

(blue dots); and ii) the area-weighted center of mass (CM) of the image (green dot). Finally,

we defined a "region of acceptability" for the centroids of the simply connected regions to be

included in the lobe count. This region was a circle, centered on CM, with a radius that was

twice as large as the diameter of the largest simply connected region. Setting this

acceptability circle allowed excluding spurious, simply connected (often very small) regions

that were far away from the CM of the STA image (yellow dots in Supplementary Fig. 1b and

d), especially in the case of poorly defined RFs. The total number of accepted centroids at the

end of this selection procedure is the lobe count reported in Fig. 5d for the different

binarization thresholds.

HMAX simulations. The structure of the HMAX model of the ventral stream has been

already described in the Results (Fig. 3) and motivated in the Discussion. For our application,

we have chosen the version of the model described in [32] and downloaded from

http://maxlab.neuro.georgetown.edu/docs/hmax/hmaxMatlab.tar. Briefly, the model is a

feedforward neural network with alternating layers of units performing: 1) either a max-

pooling (invariance-building) operation over input units with the same feature-selectivity, but

RFs having different positions/scales (C1 and C2 units; dashed lines in Fig. 3); or 2) a

template-matching (selectivity-building) operation over input units with different feature

selectivity (S1 and S2 units; solid lines). As pointed out in the Discussion, the feature

representations built by the model in the S-type layers are not learned, and there is no attempt

to maximize classification accuracy in a given discrimination task. The S1 layer is simply a

bank of Gabor filters with various orientations, spatial frequencies, positions and scales

(similar to V1 simple cells), while the S2 units are tuned to random patches of images taken

from various databases (e.g., Caltech 101), with different units having as a template the same

image patch, but at different positions and scales. Such static, hardwired architecture makes

the model very suitable to isolate the role of the max-pooling and template-matching

computations in determining the tuning for oriented gratings along a ventral-like processing

hierarchy.

To this aim, we fed as an input to the network (i.e., to the S1 layer) a set of drifting

gratings spanning the same range of directions used in the neurophysiology experiment. Each

drifting grating was decomposed as a sequence of consecutive frames, and the activations of

the units of the network in response to such frames were computed to simulate the evolution

over time of the neuronal responses. Given a unit, its preferred stimulus direction was chosen

and the power spectrum of its time-dependent (i.e., frame-dependent) response was computed

to estimate the modulation index MI. We also integrated the activation of each unit over the

whole stimulus presentation to compute its overall mean response for a given grating

direction. By iterating this procedure for each stimulus direction, we built orientation and

direction tuning curves and computed OSI and BSI values. All these indexes were computed

for a randomly selected subset of units ($n = 250$) in each layer. The resulting distributions are

those shown in Figs. 4c, 6c and 7c.

Statistical analysis. Differences between median values of two distributions were quantified

using a Mann-Whitney U-test. Differences in the faction of units above or below a certain

threshold index value (for MI, OSI, BSI or CI) were quantified using the χ^2 test for

homogeneity with one degree of freedom. When needed (i.e., in case of small sample size),

Fisher exact test was used to compare two distributions (e.g., the lobe count distributions in

Fig. 5d). Finally, in the meta-analysis shown in Fig. 8, we compared the mean fractions of

modulated (Fig. 8a) and orientation-tuned (Fig. 8b) units across primate visual cortical areas

V1, V4 and IT using a one-way ANOVA.

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Author contributions

F.B.R., G.M. and D.Z. conceived the study. G.M. designed the stimuli and implemented the

presentation protocol. F.B.R., G.M. and R.B.M. performed the experiments. F.B.R., G.M.,

R.B.M. and D.Z. analyzed the data. G.M. performed the simulations of the computational

model. F.B.R. and G.M. carried out the meta-analysis of the ventral stream literature. F.B.R.,

G.M. and R.B.M. did the artwork. F.B.R., G.M., R.B.M. and D.Z. wrote the manuscript.

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