Bagging Improves Reproducibility of Functional Parcellation of the Human Brain

Aki Nikolaidis (1), Anibal Solon Heinsfeld (1), Ting Xu (1), Pierre Bellec (2), Joshua Vogelstein (3), Michael Milham (1).

1- The Child Mind Institute, 101 East 56th Street. New York, NY 10022
2- University of Montreal, PO Box 6128 Downtown STN Montreal QC H3C 3J7 CANADA
3- Department of Biomedical Engineering, Institute for Computational Medicine, Kavli Neuroscience Discovery Institute, Johns Hopkins University 3400 N. Charles St Baltimore, MD 21218

Abstract:
Increasing the reproducibility of neuroimaging measurement addresses a central impediment to the advancement of human neuroscience and its clinical applications. Recent efforts demonstrating variance in functional brain organization within and between individuals shows a need for improving reproducibility of functional parcellations without long scan times. We apply bootstrap aggregation, or bagging, to the problem of improving reproducibility in functional parcellation. We use two large datasets to demonstrate that compared to a standard clustering framework, bagging improves the reproducibility and test-retest reliability of both cortical and subcortical functional parcellations across a range of sites, scanners, samples, scan lengths, clustering algorithms, and clustering parameters (e.g., number of clusters, spatial constraints). With as little as six minutes of scan time, bagging creates more reproducible group and individual level parcellations than standard approaches with twice as much data. This suggests that regardless of the specific parcellation strategy employed, bagging may be a key method for improving functional parcellation and bringing functional neuroimaging-based measurement closer to clinical impact.

Keywords: reproducibility, bagging, parcellation, cluster ensembles, reliability, biomarkers, striatum, thalamus, subcortical, basal ganglia, fMRI, bootstrap

1. Introduction

Understanding the brain's organization is a fundamental goal of human neuroscience (Glasser et al., 2016) and important for clinical impact (Fox & Greicius, 2010). Brain parcellations are distinct partitions in the brain that can be individual contiguous areas, or networks made up of closely interacting regions (Eickhoff, Yeo, & Genon, 2018). Parcellation of the human brain into functionally homogeneous areas has seen impressive advances in recent years on resting state and multimodal neuroimaging (Eickhoff et al., 2018), often through the use of global similarity based clustering (Bellec, Rosa-neto, Lyttelton, Benali, & Evans, 2010; Craddock, James, Holtzheimer, Hu, & Mayberg, 2012; Thirion, Varoquaux, Dohmatob, & Poline, 2014), multivariate decomposition (Beckmann, Mackay, Filippini, & Smith, 2009; Varoquaux, Gramfort, Pedregosa, Michel, & Thirion, 2011), or local gradient-based methods (Cohen et al., 2008; Glasser et al., 2016; Gordon et al., 2014; Nelson et al., 2010; Wig et al., 2014; Xu et al., 2016). Such network- and region-level parcellations have enabled a greater understanding of fundamental attributes of the brain's multi-level network structure (Bellec et al., 2015; Buckner, Krienen, Castellanos, Diaz, & Yeo, 2011; Margulies et al., 2016; Meunier, Lambiotte, Fornito, Ersche, & Bullmore, 2009; Yeo et al., 2011). Parcellations of the brain also commonly form the nodal backbone of network neuroscience studies (Hagmann et al., 2007; Zalesky et al., 2010), which have been successful in exploring the network structure of the brain and successfully predicting a wide variety of cognitive (IQ: (Finn et al., 2015; Shehzad et al., 2014); Complex Task performance: (Nikolaidis, Goatz, & Smaragdis, 2015)), developmental (Age: (Dosenbach et al., 2010; Liem et al., 2017)), physical (Aerobic fitness: (Talukdar et al., 2017)), and clinical phenotypes (Autism: (Abraham et al., 2017; Hong, Valk, Di Martino, Milham, & Bernhardt, 2018); Tourette's Syndrome: (Greene et al., 2016)), and are an essential area of research for understanding human brain organization. Unfortunately, studies suggest that the amount of scan time required to achieve desirable levels

of reproducibility and reliability appear to surpass the scan time in most clinical and cognitive

neuroscience datasets already collected or currently underway (Laumann et al. 2015; Xu et al.

2016; Zuo et al. 2019; Greene et al. 2019). As such, there is also an increasing need for methods

that can optimize the value of resting state acquisitions with insufficient data. The importance of

functional parcellations in understanding brain organization and clinical, cognitive, and

developmental phenotypes makes it critically important to assess new methods for improving their

reproducibility and reliability.

Bootstrap aggregation, a popular technique from statistics and machine learning may

assist in improving the reproducibility of functional parcellations. Bootstrapping and bootstrap

aggregation are both general parametric or nonparametric procedures used to improve statistical

inference along many dimensions, including improved estimates of certainty of an effect,

estimating p-values, and accuracy. Bootstrapping refers to resampling a dataset with

replacement, and has found a wide range of applications in science and statistics (Efron &

Tibshirani, 1994). For example, bootstrapping is used for estimating the accuracy of a sample

estimate and is based on the notion that a sample's population can be modeled by resampling.

Building on this concept, bootstrap aggregation, or bagging, was originally designed to resample

data for prediction, and to aggregate the predictions across bootstrap samples to improve

predictive performance (Breiman, 1996). Bagging is thought to reduce variability in the estimation

through averaging (prediction labels or cluster membership) over multiple resampled datasets

(Dudoit & Fridlyand, 2003). More recently, bagging has become an important technique for

ensemble clustering, which is a way of creating a final clustering by aggregating a range of cluster

solutions (Jia et al. 2011; Li and Ding 2008; Fischer and Buhmann 2003; Zhou 2012; Hong et al.

2009; Leisch 1999). In bagging for clustering, cluster partitions across all bootstrap samples form

a cluster stability matrix by recording for each pair of observations the proportion of times they

were clustered together in the bootstrap clusters (Dudoit and Fridlyand 2003; Fred and Lourenço

2008). This stability matrix is then used as input to a clustering procedure to create the final

clustering. In other words, the aggregation of cluster solutions themselves become the features

for ensemble clustering (Strehl & Ghosh, 2002).

Numerous studies outside of the imaging community (Dudoit & Fridlyand, 2003; Jia et al.,

2011; Li & Ding, 2008; Strehl & Ghosh, 2002; Zhou, 2012), and one within (Hoyos-Idrobo,

Schwartz, Varoquaux, & Thirion, 2015), have found that both: (1) within-sample instability, and

(2) sensitivity to noise inherent to the cluster optimization procedure, are significantly attenuated

by cluster ensembles generated through bagging. These and other efforts have demonstrated the

impact of bagging cluster ensembles in improving the cluster homogeneity, stability, and accuracy

of clusters (Boongoen and Iam-On 2018; Lange et al. 2004). We hypothesized that bagging

cluster ensembles may specifically improve the between sample and between session

reproducibility and reliability of individual and group parcellations as well. Given the importance

of reproducibility of parcellations as outlined above, enhancing clustering procedures via bagging

could dramatically improve reproducibility in a wide range of clinical and cognitive applications

that rely on clustering.

In the present work, we leverage the Bootstrap Analysis of Stable Clusters (BASC)

framework, and a recently developed Python extension, referred to as PyBASC. BASC is an

implementation of bootstrap aggregation for functional neuroimaging analysis that was initially

created to assess the stability of parcellations across a range of cluster resolutions and choose

the 'best' resolutions that maximize within subject and within sample parcel quality and stability

(Bellec et al., 2010). Such stability selection efforts have been demonstrated elsewhere to

improve the estimation of structure in data (Meinshausen & Bühlmann, 2010) and are particularly

well suited for choosing the number of clusters (von Luxburg, 2010). Initial efforts demonstrated

that the circular block bootstrap (CBB) was advantageous for the estimation of robust associations

between brain regions (Bellec, et al., 2008); later work focused on using CBB and bootstrapping

at the group level to demonstrate the hierarchical nature of brain networks (Bellec et al., 2010,

Bellec et al., 2015). PyBASC leverages the power of Nilearn (https://nilearn.github.io/), Scikit learn

(Pedregosa et al., 2011), and Nipype (Gorgolewski et al., 2011) to build an open source Python

package for BASC (GitHub: https://github.com/AkiNikolaidis/PyBASC; PyPI:

https://pypi.org/project/PyBASC/). PyBASC allows both standard parcellation schemes (similar to

Craddock et al. 2012), as well as bagging derived cluster ensembles as described above.

Furthermore, we extend prior work in clustering and bagging ensembles by examining how

bagged parcellations can be used to improve the reproducibility across sample, session, and

study.

Keeping in line with extensive efforts at both cortical (Bellec et al., 2010; Craddock et al.,

2012; Kelly et al., 2009; Kelly et al., 2012; Margulies et al., 2007) and subcortical parcellation

(Barnes et al., 2010; Choi, Yeo, & Buckner, 2012; Garcia-Garcia et al., 2017; Janssen, Jylänki,

Kessels, & van Gerven, 2015), we perform functional parcellation at multiple resolutions in both

cortex and subcortex to assess the impact of bagging on reproducibility and reliability of these

parcellations. While several cortical parcellations are well established (Glasser et al., 2016; Yeo

et al., 2011), subcortex is an area where parcellations are less well-studied (Choi et al., 2012;

Janssen et al., 2015). Subcortical regions are also in need of methods to improve reproducibility

and reliability given that they show connectivity with notably lower reliability than the rest of the

brain (Noble et al., 2017; O'Connor et al., 2017).

The goal of the present work is to improve the reproducibility of parcellations through the

use of bagging enhanced ensemble clusters with PyBASC. We approach the issue of bagging for

enhancing functional parcellation reproducibility across a range of parameters such as scan

length, cluster number, sample size, cluster parameters, clustering method, and region of interest.

We created parcellations of both cortex and subcortical structures using both bagging and a

standard non-bagged approach leveraging two large datasets with multiple resting state

acquisitions per participant (i.e., the Hangzhou Normal University (HNU1) from the Consortium

for Reliability and Reproducibility (Zuo et al., 2014), and the Brain Genomics Superstruct Project

(GSP) datasets (Holmes et al., 2015); see Table 1). We compare the similarity across scans,

across individuals, and across groups to evaluate standard and bagging based parcellations in their reproducibility, reliability, and individual-to-group similarity. Importantly, reproducibility is quantified in different contexts: (1) of individual level parcellations within a sample, (2) of individual and group level parcellations between samples and sessions, and (3) of parcellations between group and individual level parcellations. To accomplish this, we use the definitional framework outlined in Table 2 and Section 2.5 & 2.6. We were motivated by the COBIDAS report (Nichols et al., 2017) and broader outlines for the establishment of reproducibility in metrology and biomedical science (JCGM, 2008).

We find that bagging has a significant impact on the reproducibility of parcellations at both the group and individual level, improving reproducibility even more than doubling scan time. Bagging enhanced parcellations are also less individually variable, exemplified by (1) large decreases in both within and between individual variance of individual level parcellations, and (2) increases in both univariate and multivariate measures of reliability. We also find that bagging increases individual-to-group similarity of the parcellations, meaning group level parcellations become more representative of the individuals in the group. Bagging improves the generalizability, reproducibility, and reliability of both cortical and subcortical functional parcellations across a range of sites, scanners, samples, scan lengths, and clustering parameters. Importantly, we find this to be true regardless of the specific cluster analysis algorithm being used. These results suggest that bagging may be an important component for achieving more robust parcellations in functional neuroimaging.

2. Materials and Methods

2.1 Overview

We aimed to approach a full-scale assessment of the impact of bagging on between sample reproducibility, between session reproducibility, and between session reliability. Towards this end, we apply PyBASC, a multi-level bagging approach for functional parcellation (See Methods Section 2.4 on PyBASC).

Data Source	Sample Size	Data Length	Age	Sex	Voxel Size	TR
HNU1	30	10x 10-Minute	24.37, +/- 2.37	50/50 % F/M	3.4, 3.4, 3.4 mm	2000ms
GSP	300	2x 6-Minute	23.67, +/- 2.15	50/50 % F/M	3.0, 3.0, 3.0 mm	3000ms

Table 1: Overview of datasets used in the current study. HNU1- Hangzhou Normal University. GSP- Genomics Superstruct Project.

2.2 HNU1 and GSP Data

We assessed the impact of bagging on reproducibility of functional parcellation using the HNU1 (Zuo et al., 2014), and GSP datasets (Holmes et al., 2015). In the HNU1 dataset, 10-minute resting state scans were acquired in 30 young adults every three days for a month, for a total of 10 sessions per person. To test between session reproducibility and reliability we split the even and odd numbered sessions into 50-minute reference and replication datasets. From the 300 participants in the GSP, we created 10 groups of 30 age- and gender-matched participants to

assess within study/between sample reproducibility. Using all 300 GSP participants combined,

we also created a reference parcellation and compared it to the HNU1 replication dataset to

assess the impact of bagging on between study/between sample reproducibility.

2.3 MRI Data

2.3.1 MRI Acquisition- *HNU1. Anatomical*: 3D SPGR images were acquired on a GE 3T scanner

(General Electric, Milwaukee, WI) with an 8 Channel head coil. Flip angle: 8 Degrees. TI: 450ms,

TE: 60ms, TR: 8.06s, 180 slices, slice thickness: 1mm. Acquisition time: 5:01. *Rest*: T2* BOLD

EPI sequence, GE 3T, 8 Channel head coil. Flip angle: 90 Degrees. TE: 30ms, TR: 2000ms, 43

slices, slice thickness: 3.4 mm. Acquisition time: 10:00.

GSP Anatomical: T1 MEMPRAGE images were acquired on Siemens 3T Magnetom Tim

Trio scanner (Siemens Medical Solutions, Erlangen, Germany) with a 12 channel head coil. Flip

angle: 7 degrees. TI: 1.1s, TE:1.5 / 3.4 / 5.2 / 7.0. TR 2.2s. 144 slices, slice thickness: 1.2mm.

Acquisition time: 2:12. *Rest*: T2* BOLD epfid2d1_72 sequence, Siemens 3T Magnetom Tim Trio,

12 channel head coil. Flip angle: 85 degrees. TE: 30ms, TR: 3.0s, 47 slices, slice thickness: 3mm.

Acquisition time: 6:12.

2.3.2 Preprocessing- *Anatomical:* 1) AFNI skull stripping. 2) MNI 152 2mm template anatomical

nonlinear registration with FNIRT. 3) Data transformed to 3mm. *Functional:* 1) Transformed to 3

mm. 2) Nuisance regression applied (white matter, CSF, global signal, motion, linear, and

quadratic components of motion). 3) Friston 24-Parameter model used for volume realignment.

4) Nuisance band pass filtering between 0.01 and 0.1 Hz. 5) Spatial smoothing applied 6mm

FWHM. Preprocessing in GSP and HNU1 structural and rest data were identical with the addition

of de-spiking to the GSP resting state data. (HNU1- CPAC Version 1.0; GSP- CPAC Version 1.2).

1
2
3
<u>Figure 1 Parcellation Overview</u>- A) Outline of different steps in standard clustering approach. B)
Creating cluster ensembles through bagging follows the same overall structure as A, with the
addition of individual level time-series resampling at step 3, and bagging across individuals in step
6. Red arrows show when bootstrap resampling occurs to create multiple resampled individual
(3) and group level data (6). Blue arrows show when bootstrap aggregation happens to create
averaged individual (5) and group level data (7).
10

2.4 PyBASC Parcellation

We first apply clustering in the same manner as is commonly applied in functional parcellation

methods when not using bagging (See Figure 1; (Craddock et al., 2012; van den Heuvel, Mandl,

& Pol, 2008). 1) We start with preprocessed functional MRI data; 2) this data is transformed from

a voxel representation to a supervoxel representation through feature reduction such as Ward's

criterion based hierarchical agglomerative clustering; 3) time series for each supervoxel is

extracted, and a correlation matrix is calculated, 4) clustering is applied to extract a specific

number of clusters (K) for each individual's correlation matrix and an adjacency matrix is created,

and 5) individual level adjacency matrices are averaged together and 6) clustered again to reveal

the group level clustering.

This approach can be extended by adding bagging both within each individual's time

series and across individuals to create resampled groups, as first implemented by BASC (Bellec

et al. 2010; Figure 1B). We explain this process briefly here (See Supplementary Materials 5.1).

At the individual level, bagging is applied using a circular block bootstrap (CBB; window size =

sqrt(number of time steps)). CBB has advantages of robustness for time series modeling and

resampling compared to commonly used autoregressive models (Adolf, Baecke, Kahle,

Bernarding, & Kropf, 2011; Adolf et al., 2014; Bellec, Marrelec, & Benali, 2008; Dupré la Tour et

al., 2017; Liégeois, Laumann, Snyder, Zhou, & Yeo, 2017). We used this method on the individual

time series to create many resampled 4D functional scans for each individual, and clustering was

applied to each individual resampled 4D scan, resulting in cluster solutions for each individual

level bootstrap. These cluster solutions are transformed to an adjacency matrix and are averaged

together to create a mean adjacency matrix for each participant. We then bagged across

individuals to create resampled groups (6), which are then averaged to create the group mean

adjacency matrix (7) that is clustered to create the final parcellation (8). This multilevel bagging

approach has been previously applied in the original BASC implementation in Octave and has

been explained in greater detail elsewhere (Bellec et al., 2010; Garcia-Garcia et al., 2017); See

Supplementary Materials 5.1 for more details about PyBASC). Here we have created a python-

based implementation of this framework, PyBASC, to conduct the following reproducibility and

reliability assessments. Overall, PyBASC and BASC follow the same algorithmic structure,

however there are a few differences worth noting for the application here: 1) Dimension reduction

is conducted through a region growing algorithm in BASC, whereas in PyBASC Ward's criterion

hierarchical clustering is applied. 2) Dimension reduction is applied at the group level in BASC,

though can be at the individual or group level in PyBASC. Here we apply individual level

dimension reduction for subcortical parcellation and group level dimension reduction for cortical

parcellation to reduce computational load.

In the current work, we applied parcellation to both cortical and subcortical regions across

a range of number of clusters (Subcortical K = 10, 18; Cortical K = 7, 20, 197, 444). We chose to

apply bagging to the problem of both subcortical and cortical parcellation due to the computational

advantage of the relatively few voxels present in our subcortical masks, which enables us to

assess the impact of bagging across a wider range of parcellation parameters at a much lower

computational cost than a full cortical parcellation. We chose K = 10, and 18 for the subcortical

parcellation given our work and other literature has repeatedly shown these parcellations fit best

for the striatum and thalamus (Behrens et al., 2003; Choi et al., 2012; Garcia-Garcia et al., 2017;

Johansen-Berg et al., 2005). We chose K = 7, 20, 197, and 444 following previous analysis

exploring multi-scale parcellation with BASC (Bellec, 2013; Bellec et al., 2010).

Functional parcellations often are created with strong spatial constraints to create more

homogenous parcel shapes with smoother parcel boundaries (Craddock et al., 2012; Schaefer et

al., 2018; Xu et al 2016). In this way such constraints can be considered a form of spatial

regularization for the cluster optimization procedure, thus reducing variance by increasing bias

and therefore increasing the reproducibility of the clustering outcomes. To provide the best test

of the impact of bagging on parcellation reproducibility we use minimal spatial constraints in the

current approach, enabling parcels that are discontinuous and even bilaterally homologous. While

such an approach yields parcels with noisier boundaries than would be the case with stronger

spatial constraints, such as Craddock et al. 2012, our approach allows the parcellation a better fit

to a given sample and provides a stricter and more direct test of the impact of bagging. Notably,

we also assessed the impact of bagging across spatial constraints (Supplementary Figure 5.2.4).

Level of Generalization	Participants		MRI		Data Used	Figures
	Pop.	Sample	Scanner	Data		
Between Scan	=	=	=	X	GSP 10 groups TRT	7
Between Session	=	=	=	X	HNU Reference & Replication	8, 9,10, 11, 12, 13
Reliability	=	=	=	X	GSP 10 groups TRT HNU Reference & Replication	14, 15, 16
Within Study Between Sample	=	X	X	X	GSP 10 groups	2
Between Study Between Sample	X	X	X	X	GSP 300 HNU Replication	3, 4, 5, 6

(Left axis: Near → Far, labeled "Reproducibility")

Table 2- Group-Level Analyses. Level of Generalization depicts which type of generalizability we tested with each analysis, see Methods sections 2.5-2.6. Columns show which kind of parameters would be kept constant (=) or changed (x) across analyses in the current study.

2.5 Reproducibility

2.5.1 Concept- The definitions of concepts of reproducibility and replicability are numerous and often conflicting (Barba, 2018). We chose to follow the Joint Committee for Guides in Metrology (JCGM). This group is comprised of eight international organizations specializing in measurement, including the International Standards Organization (ISO), which the COBIDAS report follows closely (Nichols et al., 2017). According to the JCGM, Reproducibility is the similarity between the results of measurements of the same or similar measurands carried out under changed conditions of measurement (JCGM, 2008).

2.5.2 Data Requirements- The changed conditions may include the method of measurement, observer, measuring instrument, reference standard, location, conditions of use, and time. Notably, statements of reproducibility must include a description of the specific conditions changed. In other words, when discussing reproducibility, it's important to be specific about what is being changed and across which dimension(s) measurements are being reproduced. Reproducibility across sessions but not samples requires multiple assessments of the same sample and is known as between session reproducibility. Similarly, reproducibility across investigators requires different investigators but can use the same method and data, which is often referred to as computational reproducibility (Millman, Brett, Barnowski, & Poline, 2018). We extend this formal definition of reproducibility to include reproducibility across samples, which we call between sample reproducibility.

To support our tests of between sample, between session, and between scan reproducibility, we created several reference and replication datasets using the HNU1 and GSP datasets. In the HNU1 dataset, we created a test-retest dataset by combining the ten, 10-minute sessions into two five-session, 50-minute scans. Our reference and replication datasets were created through a concatenation of each participant's even and odd numbered session's respectively. To assess the interaction of bagging and length of acquired data on reproducibility, we performed parcellation across the first 3, 5, 10, 15, 20, 25, and 50 minutes of the replication

data. We split the 300 participants of the GSP data into 10 groups of 30 participants that were

age and sex matched to the HNU1 dataset, and we used these 10 groups to assess both between

sample and between scan reproducibility, given these two 6-minute scans were acquired in the

same session. We also concatenated both 6-minute sessions and used all 300 participants of the

GSP dataset to create a large reference parcellation, and we compared this reference to the

replication sets of the HNU1 data to test between sample reproducibility.

2.5.3 Testing Methods- To measure between session reproducibility, we assessed the similarity

between the reference and each of the replication datasets using spatial correlation of these group

level mean adjacency matrices, and the adjusted Rand index (ARI) of the group level cluster

labels. Given that bagged clustering is non-deterministic, we assessed the variance in our

parcellations by repeating our parcellations 20 times for each replication dataset across each

amount of scan time and bootstrap aggregation for the subcortical parcellation. For the cortical

parcellation we repeated the parcellations 10 times, with the HNU1 10-minute replication data.

Since the standard, non-bagged, clustering approach is deterministic, we needed a method to

assess the variance in between session reproducibility of the parcellations. To overcome this

issue, we created 20 new datasets for each amount of the scan lengths by resampling the 50-

minute replication dataset (See Supplementary Materials 5.1 for details on this resampling

method). We applied PyBASC without bagging across each of these 20 datasets to estimate the

variance in between session reproducibility for the standard parcellation condition.

We assessed the effect of bagging on within study/between sample reproducibility of

functional parcellation by comparing the parcellations between 10 age and sex-matched groups

of 30 participants from the GSP dataset. Since we had 10 groups, we did not need to resample

and repeat our bagged or standard parcellations as above. Each of the two 6-minute scans were

used for each group, as well as a concatenated 12-minute scan. We compared the similarity of

group level parcellations between the 10 groups for each scan length, and we compared the

parcellations of the ten groups for both 6-minute scans. Second, we assessed the effect of

bagging on between study/between sample reproducibility. We used the same 12-minute scans

from all 300 GSP participants together to create a reference parcellation. For assessing cortical

parcellation reproducibility, we compared the GSP reference to the 10-minute HNU1 data. For

assessing subcortical parcellation reproducibility we assessed the GSP parcellation against a

range of HNU1 scan lengths.

2.6 Reliability & Discriminability

2.6.1 Concept- Reliability is a metric of the inter- and intra-individual stability of a measurement

across multiple occasions (Zuo & Xing, 2014), and can be measured with different indices.

Intraclass correlation (ICC) is a descriptive statistic that relates the within individual to between

individual variance to get an indication of univariate reliability (Shrout & Fleiss, 1979).

Discriminability is a multivariate metric of reliability that takes the full set of features across all

observations into account to compute a multivariate index of reliability (Bridgeford et al. 2020;

https://github.com/neurodata/r-mgc).

2.6.2 Data Requirements- Calculating test retest reliability requires at least two observations of

the same individuals in the same group. In the current study, we compute ICC using two

measurements from each individual in both the HNU1 and GSP samples.

2.6.3 Testing Methods- We assessed whether bagging would improve both the univariate and

multivariate reliability of our functional parcellations, and how scan length would have an impact

on these results. Using the same set of functional parcellations across multiple datasets

calculated in Section 2.5 Reproducibility, namely the reference and multi-length replication

datasets, we calculated the ICC for each cell in the individual level mean adjacency matrix data,

and discriminability for the individual mean adjacency matrix as a whole.

2
3
Figure 2- Bagging Improves Reproducibility of Group Level Within Study/Between Sample
Subcortical Parcellation. We compare the parcellations from 10 groups of 30 participants from the
GSP sample to one another. The vertical dotted blue line marks the standard clustering approach
on the left, and the bagging approach on the right. The horizontal dashed red line shows the
highest mean reproducibility of the standard parcellation approach. A & B Spatial correlation
between mean group adjacency matrix of 10 GSP groups with 10 and 18 clusters. C & D ARI
between cluster labels of 10 GSP groups with 10 and 18 clusters.
11

Figure 3- Bagging Improves Reproducibility of Group Level Between Study/Between Sample
Cortical Parcellations. We compared a reference parcellation created from the 12-minute
combined scan from 300 individuals from the GSP to 10 repeated parcellations of 10 minutes of
HNU1 data. A) Spatial correlation between the group mean adjacency matrix for the GSP and
HNU1 parcellations. B) ARI between the cluster labels for the GSP and HNU1 parcellations.

<u>Figure 4- Bagging Improves Reproducibility of Group Level Between Sample Subcortical</u>
<u>Parcellations.</u> Bagging improves the reproducibility of subcortical brain parcellation between the
GSP and HNU1 datasets, though results more mixed than the cortical results. We compared a
reference parcellation created from the 12-minute combined scan from 300 individuals from the
GSP to 10 repeated parcellations of 10 minutes of HNU1 data. The vertical dotted blue line marks
the standard clustering approach on the left, and the bagging approach on the right. The horizontal
dashed red line shows the highest mean reproducibility of the standard parcellation approach. A
& B Show spatial correlation between the group mean adjacency matrix for the GSP and HNU1
parcellations for K = 10 and K = 18. C & D Show ARI between the cluster labels for the GSP and
HNU1 parcellations for K = 10 and K = 18.
12
13

2
3
Figure 5 - Visualization of Group and Individual Level Between Study Cortical Parcellations. We
show the similarity of the HNU1 parcellation to the GSP reference parcellation with K = 7 clusters
as shown in Figure 3. We use a K-nearest neighbor spatial filter on these parcellations to improve
ease of visual comparison. Notably, both the group and individual level parcellations with 400
bootstraps are closer to the GSP reference parcellation than either of the standard parcellations.
A) Group-level parcellation with standard approach, and B) bootstrapping. C) GSP Reference
parcellation. D) Individual-level parcellation with standard approach, and E) bootstrapping.

Figure 6 - Visualization of Group and Individual Level Between Study Subcortical Parcellations.
We show the similarity of the HNU1 parcellation to the subcortical GSP reference parcellation
with 10 clusters as shown in Figure 4. Both the group and individual level bootstrapped
parcellations are notably more similar to the GSP reference than either of the standard
parcellation counterparts. A) Group-level parcellation with standard approach, and B)
bootstrapping. C) GSP Reference parcellation. D) Individual-level parcellation with standard
approach, and E) bootstrapping.

3. Results

3.1 Bagging Improves Between Sample Reproducibility

Improving between sample reproducibility is key for creating generalizable scientific discovery. We assess two different levels of between sample reproducibility here: within study and between study, and we hypothesized that bagging should have a beneficial impact on both levels. As a first step, we investigated the effect of bagging on the within study/between sample reproducibility of our subcortical parcellations (Figure 2). We split the 300 GSP participants into 10 groups of 30 and computed the correlation of the subcortical parcellations group mean adjacency matrices (Figure 2 A, B), and the ARI of their cluster labels between groups (Figure 2 C, D). We found that while increasing the time of the scan from 6 to 12 minutes significantly improved reproducibility when measured by both correlation and ARI (K = 10; Correlation: Kruskal-Wallis = 58.52, df = 1, p-value < 0.0001; ARI: Kruskal-Wallis = 10.79, df = 1, p-value < 0.005), we found that the impact of bagging improved reproducibility more than increasing the scan length (K = 10; Correlation: Kruskal-Wallis = 401.26, df = 1, p-value < 0.0001; ARI: Kruskal-Wallis = 278.9, df = 1, p-value < 0.0001), indicating that the 6 minute scans could become more reproducible than scans twice as long with the use of bagging. We also found that bagging significantly decreased the variance in the reproducibility estimates for both 6 minute and 12 minute scans, but had a greater impact on the 12 minute scans (6 min ARI variance 0 vs 400 bootstraps: $F(267,267) = 0.716$, p-value < 0.01; 12 min ARI variance 0 vs 400 bootstraps $F(89,89) = 1.6712$, p-value < 0.05).

As a further test of generalizability, we tested between study/between sample reproducibility of both cortical parcellation between the GSP and HNU1 studies (Figure 3; Figure 5). These studies differ on many criteria including scanner type and population. While the GSP data was collected in the USA with Siemens 3T Magnetom Tim Trio scanners, the HNU1 data was collected in China with a GE 3T scanner. We hypothesized that bagging should not only

improve the reproducibility of the parcellations, but also that it may have an impact on the

consistency of the replication parcellations as well. We conducted a range of tests to assess these

concepts. First, using the 300 individuals from the GSP study to create a reference cortical

parcellation, we assessed the correlation of the group mean adjacency matrices (Figure 3 A), and

the ARI of the group cluster labels (Figure 3 B). We demonstrated that cortical parcellations were

more reproducible between studies using bagging; for example, for K = 444, bagging improves

ARI (Kruskal-Wallis test comparing 400 vs 0 bootstraps = 12.79; $p < 0.0005$). We also found that

bagging lowered the variance of ARI across repeated parcellations (Test of unequal variance of

ARI 0 vs 400 bootstraps: $F = 106.67$, $p < 0.0001$). This shows that the parcellations of the

replication dataset were not only more consistent with the reference dataset, but also that

repeated parcellations of the replication dataset were more consistent with each other when

bagging was used than when it was not. One of the challenges in parcellation is that as we

increase spatial scale, we tend to lose reproducibility (Arslan et al., 2018), making obtaining highly

detailed maps of the brain problematic. We find that bagged parcellations at higher resolution (K

= 197) are as reproducible as network level parcellations without bagging (K = 7; Figure 3). This

indicates that bagging also assists in achieving reproducible functional parcellations at higher

resolutions.

Third, we found that bagging had a significant impact on the between study/between

sample reproducibility of subcortical parcellation, comparing the GSP reference to the HNU1

dataset (Figure 4; Figure 6). Both correlation and ARI of the parcellations improves with scan time

from 10 to 50 minutes as expected. However, we expected that bagging would improve the

parcellation labels equally for both the 10- and 50-minute replication samples. What we found

instead, is that while both improved significantly from 0 to 400 bootstraps, the 10-minute HNU1

dataset improved much more than the 50-minute (K = 10, 10 minute: $t = -13.087$, $df = 21.389$, p-

value < 0.0001; 50 minute: $t = -3.2407$, $df = 21.75$, p-value < 0.005). When visualized (Figure 6;

Supplementary Material 5.2.1), we see this difference is largely due to the fact that both the GSP

reference and the 10-minute HNU1 scans split the bilateral caudate into two clusters, whereas

the 50-minute HNU1 parcellation did not. In fact, the 50-minute HNU1 replication and reference

data yielded a seemingly better quality parcellation overall, with less variance on the edges

between parcels, and more homotopic similarity, which can be expected given homotopic

connectivity is known to be especially high (Zuo et al., 2010). We also visualized the voxelwise

differences in parcellation labels on average over all HNU1 bootstrapped conditions and found

most differences could be found in the boundary regions between parcels (See Supplementary

Figure 5.2.1). Of note here, is that the clusters created have minimal spatial constraints applied

to them, implying that neither the cluster solutions themselves, nor the improvement in

reproducibility come from the clusters being forced into a similar spatially or anatomically

constrained configuration (Shen, Tokoglu, Papademetris, & Constable, 2013). In fact, we see

many clusters in the HNU1 50-minute Reference and Replication solution that are anatomically

distinct but functionally united bilateral homologues (i.e. the left and right putamen cluster

together, the left and right caudate cluster together, etc.).

Bootstrap Aggregates

Figure 7- Bagging Improves Reproducibility of Group Level Within Sample/Between Scan
Subcortical Parcellations. We split the 300 participants of the GSP dataset into 10 groups of 30
and compare the parcellations of their first and second functional scan to one another. The vertical
dotted blue line marks the standard clustering approach on the left, and the bagging approach on
the right. The horizontal dashed red line shows the highest mean reproducibility of the standard
parcellation approach. A & B show the improvement in bagged parcellations measured by spatial
correlation of the group mean adjacency matrix for 10 and 18 clusters respectively. C & D show
the improvement in bagged parcellations measured by the ARI of the cluster labels for 10 and 18
clusters respectively.

3 Figure 8- Bagging Improves Reproducibility of Group Level Between Session Cortical
4 Parcellations. We compared the HNU1 reference to the HNU1 replication cortical parcellation. A)
5 Spatial correlation between the group mean adjacency matrix for the reference and replication
6 parcellations. B) ARI between the cluster labels for the reference and replication parcellations.

Figure 9-Bagging Improves Reproducibility of Group Level Between Session Subcortical Parcellations. We compared the HNU1 reference to the HNU1 replication subcortical parcellations across different lengths of time. The vertical dotted blue line marks the standard clustering approach on the left, and the bagging approach on the right. The horizontal dashed red line shows the highest mean reproducibility of the standard parcellation approach. A) Spatial correlation between the group mean adjacency matrix for the reference and replication parcellations. B) ARI between the cluster labels for the reference and replication parcellations.

Figure 10- Group Bagging Alone Improves Reproducibility of Within Study/Between Session
Subcortical Parcellations. We compare the subcortical parcellations of the 50-minute replication
and reference datasets from HNU1 when only group level bagging is performed. The vertical
dotted blue line marks the standard clustering approach on the left, and the bagging approach on
the right. The horizontal dashed red line shows the highest mean reproducibility of the standard
parcellation approach. A & B show the improvement in the spatial correlation of the group level
mean adjacency matrix for K = 10 and K = 18, while C & D show the improvement in the ARI of
the group cluster labels for K = 10 and K = 18.

2 Figure 11 - Bagging Increases reproducibility of Individual Level Parcellations. Individual-level
3 bagging improves between session reproducibility of individual level parcellations across a range
4 of bagging levels and range of scan times for the HNU1 data. We compare the individual mean
5 stability matrix for each participant (A, B) and the individualized cluster labels (C, D).

Figure 12 - Visualization of Group and Individual Level Between Session Cortical Parcellations. We show the similarity of the HNU1 reference parcellation to the HNU1 replication parcellation with 7 clusters as shown in Figure 8. We use a K-nearest neighbor spatial filter on these parcellations to improve ease of visual comparison. Both the group and individual level bootstrapped parcellations are notably more similar to the HNU1 reference than either of the standard parcellation counterparts. We see notably more evidence for large-scale network similarities between the HNU1 reference and the bootstrapped parcellations at both the individual and group level, though the individual level is less obvious. A) Group-level parcellation with standard approach, and B) bootstrapping. C) HNU1 Reference parcellation. D) Individual-level parcellation with standard approach, and E) bootstrapping.

1
2
Figure 13 - Visualization of Group and Individual Level Between Session Subcortical Parcellations. We show the similarity of the HNU1 reference parcellation to the subcortical HNU1 replication parcellation with 10 clusters, as shown in Figure 9. Both the group and individual level bootstrapped parcellations are notably more similar to the HNU1 reference than either of the standard parcellation counterparts. A) Group-level parcellation with standard approach, and B) bootstrapping. C) HNU1 Reference parcellation. D) Individual-level parcellation with standard approach, and E) bootstrapping.

3.2 Bagging Improves Between Session and Between Scan Reproducibility

Whereas creating parcellations with high between sample reproducibility is key for generalizing scientific discovery, creating parcellations with higher between session and between scan reproducibility is key for decreasing uncertainty in measuring change over time, which is key for clinical and developmental neuroscience. We tested between scan reproducibility using the subcortical parcellations of the GSP dataset. We tested between session reproducibility using both subcortical and cortical parcellations of the HNU1 dataset.

First, we found that our subcortical parcellations of the GSP dataset, where we compared the effect of bagging on between scan reproducibility of 10 separate groups of 30 participants, had higher between scan reproducibility with bagging with as little as 6 minutes of data (Figure 7). This suggests that long scan times are not required for bagging to have a significantly beneficial impact on a parcellation's between scan reproducibility of the group mean adjacency matrix and cluster labels (K = 10; Correlation: Kruskal-Wallis = 14.29, df = 1, p-value < 0.0005; ARI: Kruskal-Wallis = 10.57, df = 1, p-value < 0.005).

We also found that our cortical parcellations had higher between session reproducibility with bagging in the HNU1 dataset (Figure 8; Figure 12). Comparing the K = 197 parcellation, we see significant improvements in both between session reproducibility of group mean adjacency matrices (Kruskal-Wallis = -78.86, df = 9.22, p-value = < 0.0001), and group cluster labels (Kruskal-Wallis = -33.30, df = 9.82, p-value < 0.0001). If parcellations have higher between session reproducibility on average but have high variance across repeated parcellations we might not have a good grasp on the extent to which a particular parcellation will match across time. Therefore, it's also important to minimize the variance in the between session parcellation reproducibility. We found that bagging also significantly decreases the variance in between session reproducibility of the group mean adjacency matrix (F(9,9) = 83.46, p-value < 0.0001), suggesting that the bagged parcellations are not only more reproducible (higher mean ARI), but

that this reproducibility is more stable as well (lower ARI variance). We also find that bagged

parcellations at higher resolutions are more reproducible than network-level parcellations without

bagging (K = 7; Figure 8). This replicates our earlier findings (Figure 3), that bagged parcellations

enable robust investigations of brain organization at higher spatial scales.

Finally, we tested the effect of bagging on the between session reproducibility of

subcortical parcellations in the HNU1 dataset (Figure 9; Figure 13). We found that scan length

had a highly significant impact on the between session reproducibility of parcellations. For

instance, comparing 5- and 50-minute group mean adjacency matrix correlation and cluster label

ARI with 0 bootstraps (K = 10; Correlation: Kruskal-Wallis = 14.14, df = 1, p-value < 0.0005; ARI:

Kruskal-Wallis = 12.18, df = 1, p-value < 0.0005), and with 400 bootstraps (K = 10; Correlation:

Kruskal-Wallis = 29.27, df = 1, p-value < 0.0001; ARI: Kruskal-Wallis = 29.27, df = 1, p-value <

0.0001). Notably, the impact of time was enhanced in the bagging condition, suggesting bagging

and scan time can work synergistically to provide parcellations with high between session

reproducibility. We also found that while between session reproducibility was improved with

bagging, these reproducibility estimates for shorter scan times were not improved as was the

case with longer datasets (10 minutes; K = 10; Correlation: Kruskal-Wallis = 29.27, df = 1, p-value

<0.00001 ; ARI: Kruskal-Wallis = 1.00, df = 1, p-value > 0.05). We also visualized the voxelwise

differences in parcellation labels on average over all HNU1 bootstrapped conditions and found

most differences could be found in the boundary regions between parcels, along a dorsal-anterior

ventral-posterior gradient (See Supplementary Materials 5.2.2), supporting the existence of small

scale gradients in thalamic functional organization (Lambert, Simon, Colman, & Barrick, 2017).

We also see that the improvement in between session reproducibility from bagging is

significantly greater than increasing scan length. For example, for the standard clustering

condition, increasing the scan time from 20 minutes to 50 minutes does not yield a significant

improvement in between session reproducibility of group mean adjacency matrix correlation or

ARI (K = 10; Correlation: Kruskal-Wallis = 2.90, df = 1, p-value > 0.05; ARI: Kruskal-Wallis =

0.797, df = 1, p-value > 0.05), but increasing the bagging from 0 to 400 has a significant effect on

the between session reproducibility of the 20-minute data (K = 10; Correlation: Kruskal-Wallis =

29.27, df = 1, p-value < 0.0001; ARI: Kruskal-Wallis = 17.58, df = 1, p-value < 0.0001). This

demonstrates that bagging can improve reproducibility even more than doubling scan time,

replicating our previous findings with the between-sample reproducibility in the GSP dataset

(Figure 2). We also found that bagging had a significant impact on reducing the variance in

between session reproducibility across multiple parcellations, replicating our results with the

cortical parcellation (20 Minutes; K = 10; Correlation: F(19,19) = 311.14, p-value < 0.0001; ARI:

F(19,19) = 9.7003, p-value < 0.0001). While the cortical parcellation demonstrated that only 10

minutes of data was needed for bagging to improve between session reproducibility in the HNU1

data (Figure 8), with the subcortical parcellation we saw that bagging did not improve the

reproducibility for less than 20 minutes of data (Figure 9). This may be due to random elements

of sampling those first 3, 5, 10, or 15-minute portions of the HNU1 dataset, or differences in the

parcellation favored by lower amounts of data compared to higher amounts, as we saw in

comparing the HNU1 50-minute parcellation to the GSP 12-minute reference parcellation in

section 3.1.

We found that bootstrapping led to significant improvements in the reproducibility of

individual level subcortical parcellations (Figure 11). Overall we saw that doubling scan time and

using bootstraps led to significant improvements in reproducibility of individual level parcellations

as measured by both spatial correlation (K = 10; Doubling scan time Kruskal-Wallis test effects

between > 39 for all scan lengths; Using bootstraps Kruskal-Wallis test effects > 720 for all scan

lengths) and ARI (Doubling scan time Kruskal-Wallis test effects > 26 for all scan lengths; Using

bootstraps Kruskal-Wallis test > 99 for all scan lengths), and these improvements were consistent

across all scan lengths (all p< 0.0005). Notably, we saw that bagging improved individual-level

reproducibility more than doubling scan time as measured by spatial correlation for all time

lengths, and as measured by ARI for scan lengths over 10 minutes. Furthermore, we replicated

this effect in our cortical parcellation as well. We find that in our cortical parcellation, bagging

significantly increases individual-level reproducibility as measured by spatial correlation of

adjacency matrices and ARI of cluster labels across all cluster levels (all p < 0.00005; Kruskal-

Wallis test: K = 7; Corr: 389.19, ARI: 200.55; K = 20; Corr: 433.73, ARI: 415.41, K = 197; Corr:

158.35, ARI: 449.25; K = 444; Corr: 86.48; ARI: 449.25). This is key for many approaches aiming

to improve individual level parcellation (Gordon et al., 2017; Kong et al., 2019; Laumann et al.,

2015; Xu et al., 2016).

Importantly, we also find that even bagging at the group level alone is enough to improve

the between session reproducibility of the functional parcellations (Figure 10). This shows that

individual level parcellations that are not bagging-enhanced can be bagged to improve the group

level representation. This finding is important for other multi-level cluster estimation problems,

such as diffusion weighted parcellation, which may benefit from the addition of group level

bagging (Glasser et al., 2016; Klein et al., 2007; Mars et al., 2011).

Notably, we also tested the impact of spatial constraints on the effect of bagging on

parcellations (Supplementary Results 5.2.3). Spatial constraints are an important consideration

when creating any functional parcellation, without spatial constraints the clustering algorithms find

groups of voxels with the most similar activation patterns regardless of their spatial distribution.

The addition of spatial constraints moves the clustering algorithm to favor voxels that neighbor

the cluster over others. If constraints are strong enough, anatomically disconnected parcels are

not possible and the shape of parcels will be driven more by the spatial constraint than the actual

underlying functional connectivity. Given that existing functional parcellation techniques use a

wide range of spatial constraint approaches, we also varied the spatial constraints employed here

to test if bagging would improve the reproducibility of parcellations across different spatial

constraint criteria. We found that bagging improves subcortical parcellation between session

reproducibility when considering fully spatially constrained clustering approaches as well

(Subcortical; K = 10; Correlation: Kruskal-Wallis = 29.27, df = 1, p-value < 0.0001; ARI Kruskal-

Wallis = 29.27, df = 1, p-value < 0.0001).

Finally, we also assessed the generalizability of the impact of bagging across functional

parcellation techniques. We included an assessment of the impact of bagging on the between

session reproducibility of subcortical parcels (K = 10) while using spectral clustering rather than

Ward's criterion based hierarchical agglomerative clustering (Supplementary Figure 5.2.5).

Replicating our other results with Ward's criterion based hierarchical agglomerative clustering

(Figure 9), we found that bagging also improved the between session reproducibility using

spectral clustering (Subcortical; 20 minutes; K = 10; Correlation: Kruskal-Wallis = 68.4, df = 4, p-

value < 0.0005; ARI: Kruskal-Wallis = 10.48, df = 4, p-value < 0.05; 50 minutes; Correlation:

Kruskal-Wallis = 85.72, df = 4, p-value < 0.0005; ARI: Kruskal-Wallis = 59.52, df = 4, p-value <

0.0005). This demonstrates that the bagging enhanced improvements in reproducibility

generalize across clustering methods.

Figure 14 - Bagging Improves ICC of Subcortical Parcellations. A, B, C show the top 50%, 75%, and 95% ICC values for the individual level mean adjacency matrices in the 10 GSP groups. D and E show the mean squared error within individuals and between individuals respectively. We see that bagging improves ICC. It also has a dramatic impact on both within individual variance (MSE) and between individual variance (MSR), with samples with the smallest drop in MSR showing the greatest pickup in ICC.

1
2 Figure 15-Bagging Improves Multivariate Reliability in Subcortical Parcellation. Figure A and B
3 show the discriminability results for the subcortical parcellation for K = 10 and K = 18 respectively.
4 The dotted blue line shows the standard clustering approach on the left, and the bagging approach
5 on the right. The dashed red line shows the top mean performance for the non-bagged
6 parcellations. Bagging leads to improved discriminability for longer scan times.
7

1
2
Figure 16 - Bagging Increases Individual-to-Group Similarity of Parcellations. Overall this figure
shows how bagging improves individual-to-group similarity between parcellations. The dotted
blue line shows the standard clustering approach on the left, and the bagging approach on the
right. The dashed red line shows the highest mean similarity of the standard parcellation
approach. A & B show the improvement in correlation between the group-mean adjacency matrix
and each individual's mean adjacency matrix for the K = 10 and K = 18 subcortical parcellation
respectively. C & D show the improvement of the ARI between the cluster's labels of the group
and individual level parcellations.

3.3 Bagging Improves Univariate and Multivariate Reliability

We found that bagging led to improvements in univariate estimates of reliability calculated with ICC of the voxel-wise mean adjacency matrices (Figure 14 A,B,C). Each of the entries in these matrices is the number of times across individual level bootstraps that two voxels are put into the same cluster. As such, the individual mean adjacency matrix is a representation of the average clustering solution across bootstrap aggregations for a given individual. ICC is calculated based on the relative size of variance between individuals compared to variance within individuals. We see that bagging led to large decreases in both between individual variance (MSR), and within individual variance (MSE; Figure 14). Notably, the decrease in MSE is slightly higher than the decrease in MSR, leading to a rise in ICC (Figure 14 D,E). In this case, ICC does not capture that bagging leads to a ten-fold decrease in variance, both within and between individuals' individual level parcellation estimates.

Motion can be a source of highly reproducible signal in MRI data and can highly influence estimates of reliability (Power, Barnes, Snyder, Schlaggar, & Petersen, 2012; Yan et al., 2013). We wanted to make sure the impact of bagging wasn't being driven by motion, and so mean framewise displacement was regressed out from each individual mean adjacency matrix and ICC, MSE, and MSR were calculated. As was the case without motion regression, here we see that bagging improves the ICC, and reduces the MSE and MSR of parcellations (Supplementary Materials 5.2.3).

The individual voxel-voxel ICCs were moderate, reflecting that each of the voxel-voxel relationships that make up the individual parcellations are not highly statistically reliable; however, it is still possible that when taken as a whole, the parcellation patterns in these adjacency matrices would be reliably distinct between individuals. We tested this using the multivariate metric of reliability called discriminability (Figure 15). This method allows us to consider the extent to which individual parcellation patterns are unique to that individual compared to the rest of the group.

Discriminability of the parcellations for the standard clustering approach was heavily impacted by the amount of data acquired and was quite high for 25 and 50 minutes of data (25-minute mean = 0.761; 50-minute mean = 0.817). We found that discriminability was significantly increased through bagging but not for all lengths of data. It seems that the individual level signals were not strong enough in 3-15 minutes of data to improve the discriminability of parcellation through bagging in the HNU1 data (all $p > 0.05$); however, we did see significant improvements from 0 to 400 bootstraps for 20 minutes (Kruskal-Wallis = 7.18, df = 1, p-value < 0.01), 25 minutes (Kruskal-Wallis = 29.44, df = 1, p-value < 0.0001); and 50 minutes (Kruskal-Wallis = 24.58, df = 1, p-value < 0.0001), showing individual parcellations became even more highly discriminable for 20 (mean = 0.71), 25 (mean = 0.89), and 50 (mean = 0.92) minutes.

Finally, when making generalizations from group level information to the individual, it's critically important that the group level information is representative of the individual (Adolf & Fried, 2019; Fisher, Medaglia, & Jeronimus, 2018). Such individual-to-group alignment is critical for deploying any group-defined models on individual level data, and as such is central for any kind of biomarker discovery process. Given that recent work has demonstrated that individual level brain networks can differ substantially from group level estimates (Gordon, Laumann, Adeyemo, & Petersen, 2015; Laumann et al., 2015), we wanted to test whether bagging could improve the individual-to-group similarity of parcellation, improving their potential for scientific and clinical applications (Figure 16). We found that bagging led to significantly more generalizable parcellations (20 minute parcellation; 0 vs 400 bootstraps; K = 10; Correlation: Kruskal-Wallis = 800.81, df = 1, p-value < 0.0001; ARI: Kruskal-Wallis = 248.43, df = 1, p-value < 0.0001), and increasing scan time did as well (K=10; Correlation: Kruskal-Wallis = 50.99, df = 1, p-value < 0.0001; ARI: Kruskal-Wallis = 16.59, df = 1, p-value < 0.0001). We also found that bagging led to an overall decrease in the variance of the individual-to-group similarity (K = 10; Correlation: $F(599,599) = 0.56$, p-value < 0.0001; ARI: $F(1199,1199) = 0.85$, p-value < 0.01), but this decreased variance was less pronounced here than in other analyses.

3.4 Characterizing Parcellations

Understanding how well parcellations map onto one another is an important element of assessing the likelihood of brain network results to generalize from one study to another. We assessed the extent to which our parcellations differed from one another and popular reference atlases. For example, we found that the differences between the HNU and GSP subcortical parcellations were most pronounced in the transition zones between parcels (Supplementary Figure 5.2.1), in particular we found the boundaries between the pallidum and putamen, and anterior superior thalamus to posterior inferior thalamus to be the source of greatest difference in the parcellations in the two datasets. Notably these differences were robust with both the 10 minute and 50-minute HNU data. Moreover, we replicate these areas of high differentiability between the HNU reference and replication datasets as well.

We also assessed the extent to which our subcortical parcellation aligned with previously established thalamic and striatal parcellations and we found that bagging neither improves nor reduces alignment between our subcortical parcellations and the FSL Harvard Oxford 3-cluster striatal solution and the FSL Harvard Oxford probabilistic 7-cluster thalamic parcellation (ARI: Kruskal-Wallis = 2.40, df = 4, p-value > 0.05). We also assessed the extent to which our cortical parcellations aligned with the Yeo and BASC atlases for K = 7. We found that bagging improved alignment for the Yeo atlas (ARI: Kruskal-Wallis = 5.86, df = 1, p-value < 0.02, but not for the BASC atlas (ARI: Kruskal-Wallis = 0.14, df = 1, p-value > 0.05). Notably our parcellations aligned with these atlases at level similar (ARI 0.2-0.3) to what would be expected comparing a wide range of atlases with different masks, samples, clustering parameters, variability in volume/surface alignment, etc.*,* as parcellations with high similarity typically share many of these attributes (Myers et al., 2019). To understand the parcel distribution across the cortex and subcortical regions we also assessed the laterality of our parcels. The laterality of a parcellation

is partially a function of the source of variance of the parcellation. For example, in some cases subcortical parcellations are conducted based on their connectivity to bilateral cortical networks (Choi et al., 2012), in which case the parcels may be mostly or exclusively bilateral, because the parcellation is segregating them with respect to their association to a relatively symmetric signals across hemispheres of cortex (Yeo et al., 2011; Bellec et al., 2015). In other cases, such as those when the subcortical areas are parcellated based on the similarity of within-region time series (Kim, Park, & Park, 2013), differences between right and left hemispheres may result in lateral differences in the parcellation, as is the case in our subcortical parcellation here. We found that over 20 repeated parcellations of the subcortical regions (20-minute HNU replication data; K = 10) about half of the parcels spanned both hemispheres (40.4%), aligning with prior work (Kim, Park, & Park, 2013). We also found that in 10 repeated parcellations of the cortex (10-minute HNU replication data; K = 7) most of the parcels were bilateral (82.9%), which aligns with previous results as well (Yeo 2011, Bellec et al., 2015). Notably we found that bootstrap aggregation did not change the number of bilateral parcels in either parcellation scheme (Subcortical: Kruskal-Wallis = 7.98, df = 4, p-value > 0.05; Cortical: Kruskal-Wallis = 0.0089, df = 1, p-value > 0.05).

4. Discussion

4.1 Overview

Our analyses revealed that bagging improves the between sample reproducibility of group level functional parcellations, and that this effect generalizes across multiple subsamples, clustering parameters, and clustering algorithms. Furthermore, we replicate these effects in both cortical and subcortical parcellations. In many cases, bagging improved reproducibility more than doubling scan time. As such, bagging appears to be a valuable means of bringing down data requirements for the reproducible study of functional brain organization. Bagging enhanced parcellations were also more reproducible and reliable at the individual level, with an order of

magnitude decrease in the MSE and MSR of individual level parcellations and significant

increases in univariate and multivariate reliability. With twenty or more minutes of data we saw

increases in discriminability for individual level parcellations that were already highly

discriminable. We saw bagging driven increases in between session individual level

reproducibility across all scan lengths and both spatial correlation and ARI metrics. This implies

that the highly detailed, individual-specific attributes of parcellations can be further enhanced

through bagging. We found that higher parcel number was associated with lower group level

reproducibility, and we found bagging alleviated some of this decrease in reproducibility, with

more detailed bagged parcellations (K = 197) being as reproducible as less detailed, network-

level non-bagged parcellations (K = 7). This suggests that bagging may be especially useful for

achieving acceptable reproducibility when moving towards finer spatial scales. We found that

bagging enhanced parcellations also had higher between session and between scan

reproducibility. This suggests that bagging enhanced parcellations are better suited for within-

sample repeated measures that are commonly used in intervention or other longitudinal studies

in clinical and cognitive neuroscience. Critically, this also demonstrates that our results generalize

from low resolution "network-level" clustering to the more detailed "parcel-level" clustering with

hundreds of regions. Finally, we found that bagging improved individual-to-group similarity of

parcellations, which is key for minimizing parcellation mismatch and as a result, the potential for

artifactual findings. Overall, our findings indicate that bagging enhanced parcellations: 1)

outperform the standard approach on a wide variety of reproducibility and reliability indices, and

2) should be considered for further implementation in cutting-edge cluster and gradient-based

parcellation and other approaches for potential improvements in making more robust

measurements of the connectome (Glasser et al., 2016; Laumann et al., 2015; Schaefer, Kong,

& Yeo, 2016; Xu et al., 2016).

4.2 Why Bagging Works

Both supervised and unsupervised machine learning methods suffer from variability of estimation that are inherent to aspects of the models themselves (Tumer & Ghosh 1999). For example, K-means is known to be unstable and sensitive to outliers (Li et al., 2011). Furthermore, when working in high dimensional spaces, as is often the case with clustering, variability in model estimation also arises due to the curse of dimensionality (Friedman, Hastie, & Tibshirani, 2001). As distances are computed in more dimensions, the density of sampling within each dimension also decreases. This sparsity of observations per dimension leads to increased variability in model estimation for a given sample or across samples. This variability in sampling means that relatively small perturbations in the either the sample, distance metrics used by the clustering algorithm, or clustering parameters, can lead to significant variability in the cluster outcomes. Detailed review of different parcellation techniques shows that while none are necessarily superior across all conditions, they can be quite different from one another (Arslan et al., 2018; Kleinberg, 2003; Priebe et al., 2019).

To overcome this variability, aggregating over multiple resampled datasets can provide a more generalizable model. When assessing a range of models, each individual model captures different elements of the structure of the data. Even if the best model were selected, important information contained in the results of the discarded, "non-optimal" models may be lost. Bagging enables the final decision to be made using information from all models collected across a range of resampled datasets, thereby mitigating this loss of information (Tumer & Ghosh, 1999). This effect of model aggregation has been well understood in the supervised learning literature (Breiman, 2001; Krogh & Vedelsby, 1995; Tumer & Ghosh, 1999), and has more recently been shown to provide similar benefits in unsupervised domains as well (Hu & Yoo, 2004; Lancichinetti & Fortunato, 2012; Strehl & Ghosh, 2002). In order for the aggregated models to improve performance, they must be different from one another (Boongoen & Iam-On, 2018; Krogh & Vedelsby, 1995; Kuncheva & Hadjitodorov, 2004), and the diversity of the aggregated models is

linked to the benefits seen through aggregation (Breiman, 2001; Hadjitodorov, Kuncheva, & Todorova, 2006). By using a multilevel bagging approach in the current work, we are able to capture information from all the variability within individuals and across individuals. We see that both levels contribute to improved parcellation reproducibility due to their ability to aggregate over different non-overlapping sources of variance.

Beyond nuisance signals (e.g., head motion, respiration, cardiac variation), the largest source of within-individual variance likely comes from the dynamic nature of functional connectivity (Chang & Glover, 2010; Hutchison et al., 2013). One possibility is that bagging may be improving parcellation stability by making the final clustering representative of the most dominant and stable trends in the data. With a clearer model of the dominant or central tendency of connectivity patterns in a brain region, bagging seems to prevent small perturbations in the data from having outsized effects on the parcellation results. We believe this contributes to the ability of bagging to improve parcellation reproducibility across scans, sessions, samples, and scanners.

Variability between parcellations also arises due to specific biases inherent within each clustering algorithm. While the field has not established any 'best' technique for functional parcellation (Arslan et al., 2018) or clustering in general (Kleinberg 2003; Priebe et al. 2019), bagging does not rely on any particular clustering technique. Though we demonstrate the impact of bagging in clustering here, bagging can be also applied in a wide range of other functional parcellation approaches (i.e. multivariate decomposition, gradient-based parcellation). With continuing advances in functional and multi-modal parcellations, bagging can be employed in new methodological approaches to continually improve parcellation reproducibility, reliability, and individual-to-group similarity. There may also be other ways in which ensemble methods and bagging can be used to improve the generalizability of functional parcellations and other MRI approaches that use clustering (Blumensath et al., 2013; Craddock et al., 2012). For example, prior work has demonstrated the utility of using clustering for tissue class segmentation in lesion

detection (Bosc et al., 2003; Juang & Wu, 2010); these efforts may be furthered by the use of cluster ensemble methods for detecting and evaluating differences lesions more reproducibly across samples and timepoints.

4.3 Improving Reproducibility

Within the scope of human neuroscience, the reproducibility of functional parcellations is especially important. Parcellations have a significant impact on the sensitivity of the connectome to phenotypic variables (Abraham et al., 2017), and there are key issues that arise when parcellations vary in their fit across groups and individuals. For example, recent work has demonstrated that up to 62% of the variance in the edges of a connectome can be explained by the alignment of the reference parcellation to the data in question (Bijsterbosch et al., 2018). This is troublesome because when parcellations do not generalize well between samples, the resulting connectome edges will conflate differences between group network structure with differences in underlying parcellation fit (Zuo & Xing, 2014). This leads to purported markers of psychiatric illness failing to reproduce, and therefore limiting production of biomarkers in psychiatry. When considering failures to replicate (e.g., (Dinga et al., 2018; Drysdale et al., 2017), it is important to consider potential limitations in the generalizability of the template parcellation applied across samples. There are a multi-faceted set of study-related differences that may exist between studies that have created the most commonly used brain atlases. This includes the differences in the kind of data acquired, including number of participants, the length of MRI scans, acquisition parameters, and scanner type. More generally, the composition of study samples may differ considerably on a range of phenotypic variables including age, sex, socioeconomic status, cognition and psychopathology (Falk et al., 2013). When parcellations are not sufficiently generalizable, it becomes more difficult to assess whether differences in functional connectivity between individuals or groups are due to inherent differences in connectivity strength between

areas, or differential fit of a parcellation. In this way, reproducible parcellations are essential for creating reproducible relationships between functional connectivity estimates and behavioral, cognitive, or clinical variables. Our finding that bagging improves parcellation reproducibility at both the group and individual level suggests bagging may be a key element to creating maps of functional organization that allow for robust estimations of brain-behavior relationships.

4.4 Lowering Data Requirements

We found that bagging enhanced parcellations allowed us to lower our minimum data requirements for generalizable functional parcellations. There are many efforts that have demonstrated that robustness and generalizability of functional neuroimaging measurement are increased considerably by increasing the length of the fMRI scan to 25 or more minutes (Elliott et al., 2019; Laumann et al., 2015; Xu et al., 2016). However, this length of time may not be appropriate for some clinical communities, as long scan times are not feasible in many developing or patient populations. Furthermore, many currently existing datasets in clinical populations have between 5-10 minutes of scan time, such as the 1000 Functional Connectomes Project (http://fcon_1000.projects.nitrc.org/fcpClassic/FcpTable.html), GSP, ABIDE I, ABIDE II and PING datasets (Di Martino et al., 2017; Di Martino et al., 2014; Jernigan et al., 2016). Therefore, finding methods to increase the stability of functional imaging without increasing scan time may assist in providing datasets of clinical populations more appropriate parcellations for their shorter scan times. Our results suggest that bagging may be a useful technique for creating more generalizable functional parcellations with less data.

4.5 Better Individual-to-Group Generalization

Bagging enhanced parcellations also have greater individual-to-group similarity compared to the standard parcellation procedure. Individual-to-group generalization is key for any scientific models attempting to make individual level inferences based on group level models or estimations. Given

that an individual system may be unique in ways that share little relationship to group models

(Fisher et al., 2018), and extensive individual-variation has been demonstrated in functional

networks (Laumann et al., 2015; Xu et al., 2016), it's also critical that if group models are used,

they are as representative of each individual in the group as possible. In other words, individual-

to-group representativeness is critical to make accurate assessments of individual level functional

connectivity. Otherwise, within group differences between individuals in edgewise connectivity will

also be the result of the parcellation fit, rather than actually the functional connection of interest

(Bijsterbosch, Beckmann, Woolrich, Smith, & Harrison, 2019; Bijsterbosch et al., 2018). This

brings the validity of the resulting brain-behavior relationships into question, as the maps being

compared are assumed to be equivalent but are not mapping the territory equally well. Our results

demonstrate that bagging may at least partially alleviate these issues by increasing the similarity

of individual-to-group parcellations, thereby leading to more valid brain-behavior estimation.

4.6 Improved Individual Level Parcellations

We find that bagging improves reproducibility of individual level parcellations. With extensive

recent efforts focusing on the importance of developing robust parcellations at the individual level

(Gordon et al. 2015; Salehi et al. 2020; Xu et al. 2016), this finding is particularly important for

improving estimation of brain-derived individual differences. Our findings demonstrate that

bagging leads to a ten-fold decrease in the variance of individual level parcellations between

sessions, and a nearly ten-fold decrease in the variance of parcellations between individuals as

well. Decreasing individual variance in parcellation over time implies that bagging enhanced

parcellations may be more able to replicate individual level parcellation patterns in the presence

of noise. Lower variance between individuals suggests that bagging enhanced parcellations bring

individuals closer together, potentially removing irrelevant differences between individuals in

parcellation patterns. This interpretation is supported by our findings showing that with enough

scan time, bagging enhanced parcellations also produce parcellations that are more

discriminable, meaning that the individual-specific parcellation patterns are enhanced. Discriminability is a key criterion for distinguishing between individuals and groups on the basis of phenotypic differences. Developing methods that enhance the discriminability of existing data enables greater sensitivity and understanding of brain-behavior relationships. By making parcellations that more accurately represent the individual, it may be possible that bagging enhanced parcellations also result in functional network edges and other metrics that are more reliable, discriminable, and are more sensitive to brain-behavior relationships as well.

4.7 Improved Within Sample Repeated Measures

Assessing change over time relies on within sample reproducibility, at both the individual and group levels. Studies of brain development create accurate phenotype-brain relationships by using large samples to overcome variability due to measurement error (Volkow et al., 2018). However, for cognitive or clinical interventions studies (Anguera et al., 2013; Nikolaidis, Voss, Lee, Vo, & Kramer, 2014; Oelhafen et al., 2013), collecting such large samples is completely unfeasible. Therefore, creating methods that improve the between session reproducibility of neuroimaging measurements may increase sensitivity of analysis to intervention related changes. By decreasing variance between individuals, within individuals, and across repeated measures, we create parcellations that may be better suited to pick up individual differences in functional connectivity that are driven by an effect of interest. This is an essential point for improving reproducibility of functional maps of the brain and bringing functional MRI closer to clinical impact.

4.8 Limitations

There are a large range of optimizations that may further improve parcellation reproducibility that were not investigated in the current work. For example, there are several preprocessing choices that may impact the reproducibility of parcellations, such as registration optimization, denoising parameter selection, and exclusion of global signal regression. While examinations of these

optimizations are outside the scope of the present work, they may have important interactions

with bagging that could have an impact on the parcellation improvements we see here. We also

note that our parcellations did not align very highly with established subcortical and cortical

parcellations. It's important to note that different techniques all produce inherently different

parcellation schemes due to differences in surface/volume brain alignment, cluster number,

regions of interest used, and cluster parameters. Furthermore, the current work has noteworthy

limitations on the samples chosen. We only used healthy young adults in both samples;

considering how to deal with the presence of meaningful between individual differences (e.g.,

development status, clinical status) when bagging in more heterogeneous samples requires

further work. Another limitation of the current study is that we did not exhaustively test the space

of cluster methods, which are known to vary in their reproducibility (Arslan et al., 2018), even

though this is possible with PyBASC (See Supplementary Materials 5.1). Bagging and cluster

ensembles are notable for being agnostic to clustering technique and have been successfully

demonstrated in a wide range of clustering techniques however, and we feel this limitation is

notable but not a significant one. Finally, the bagging procedures executed in the current work

add computational requirements to the creation of parcellations. Therefore, when very large

datasets or very high-resolution functional data are used, this technique may not be technically

feasible. This may change in the future as more advanced computational resources become

available. There are a range of other optimizations yet to be investigated, and the current work is

just one step in that direction.

4.9 Future Directions

In the age of the 'replication crisis' in neuroimaging, methods to improve the reproducibility of our

neuroimaging measurement are absolutely essential. Bagging for improved cluster stability is not

a new technique, nevertheless its rarely used in functional parcellation and clustering in

neuroimaging. We hope that the current effort has addressed a lack in the extant literature on the

benefits of bagging on between sample and between session reproducibility of cluster estimation.

While the current effort aimed at establishing the role of bagging in improving reproducibility and

reliability of functional parcellations, the number of tests were far from exhaustive. There are more

ways that bagging and cluster ensembles could be leveraged to improve measurements of the

brain. For instance, varying and aggregating over a range of time series window lengths, cluster

techniques, or resampling methods may lead to better individual level and group level estimates.

Some research has demonstrated that selecting diverse sets of cluster solutions for aggregation

can outperform simply aggregating all cluster solutions (Hadjitodorov et al., 2006). Such a

diversity selection approach could also be employed in a similar context and may likely improve

reproducibility and reliability of the cluster solutions as well. Given that bagging improves these

qualities in parcellations, it's possible that bagged parcellations may also show improved

reproducibility and reliability of edgewise functional connectivity. Furthermore, these edges may

also be more sensitive to phenotypic differences between people and groups, and these

considerations should be explored in future work.

Acknowledgements: We would like to thank Lei Ai and Yu Tong for their assistance with the
GSP and HNU1 datasets. We would also like to thank the extensive open science infrastructure
that supported the creation of this work, in particular the OHBM and Brainhack communities for
their input and support during the creation of this project. We would like to thank Xinian Zuo and
Randy Buckner and the teams behind the creation and release of the HNU1 and GSP datasets,
as well as the participants involved in both. We would also like to thank the teams involved in the
creation of Nilearn and Scikit Learn, two programming resources that have been invaluable to the
current work.
24
25 **Funding:** AN is supported by R21MH118556-02 and a NARSAD Young Investigator Award from
26 the Brain and Behavior Research Foundation.

References

Abraham, A., Milham, M. P., Di Martino, A., Cameron Craddock, R., Samaras, D., Thirion, B., & Varoquaux, G. (2017). Deriving reproducible biomarkers from multi-site resting-state data: An Autism-based example. *NeuroImage*, Vol. 147, pp. 736–745. https://doi.org/10.1016/j.neuroimage.2016.10.045

Adolf, D., Baecke, S., Kahle, W., Bernarding, J., & Kropf, S. (2011). Applying multivariate techniques to high-dimensional temporally correlated fMRI data. *Journal of Statistical Planning and Inference*, *141*(12), 3760–3770.

Adolf, D., Weston, S., Baecke, S., Luchtmann, M., Bernarding, J., & Kropf, S. (2014). Increasing the reliability of data analysis of functional magnetic resonance imaging by applying a new blockwise permutation method. *Frontiers in Neuroinformatics*, *8*, 72.

Adolf, J. K., & Fried, E. I. (2019). [Review of *Ergodicity is sufficient but not necessary for group-to-individual generalizability*]. *Proceedings of the National Academy of Sciences of the United States of America*, *116*(14), 6540–6541.

Anguera, J. A., Boccanfuso, J., Rintoul, J. L., Al-Hashimi, O., Faraji, F., Janowich, J., … Gazzaley, A. (2013). Video game training enhances cognitive control in older adults. *Nature*, *501*(7465), 97–101.

Arslan, S., Ktena, S. I., Makropoulos, A., Robinson, E. C., Rueckert, D., & Parisot, S. (2018). Human brain mapping: A systematic comparison of parcellation methods for the human cerebral cortex. *NeuroImage*, *170*, 5–30.

Barba, L. A. (2018). Terminologies for Reproducible Research. Retrieved from http://arxiv.org/abs/1802.03311

Barnes, K. A., Cohen, A. L., Power, J. D., Nelson, S. M., Dosenbach, Y. B. L., Miezin, F. M., …
  Schlaggar, B. L. (2010). Identifying Basal Ganglia divisions in individuals using resting-state
  functional connectivity MRI. *Frontiers in Systems Neuroscience*, *4*(June), 18.

Beckmann, C. F., Mackay, C. E., Filippini, N., & Smith, S. M. (2009). *Group comparison of
  resting-state FMRI data using multi-subject ICA and dual regression*. 181.

Behrens, T. E. J., Johansen-Berg, H., Woolrich, M. W., Smith, S. M., Wheeler-Kingshott, C. A.
  M., Boulby, P. A., … Matthews, P. M. (2003). Non-invasive mapping of connections
  between human thalamus and cortex using diffusion imaging. *Nature Neuroscience*, Vol. 6,
  pp. 750–757. https://doi.org/10.1038/nn1075

Bellec, P. (2013). Mining the Hierarchy of Resting-State Brain Networks: Selection of
  Representative Clusters in a Multiscale Structure. *2013 International Workshop on Pattern
  Recognition in Neuroimaging*, 54–57. ieeexplore.ieee.org.

Bellec, P., Benhajali, Y., Carbonell, F., Dansereau, C., Albouy, G., Pelland, M., … Orban, P.
  (2015). Impact of the resolution of brain parcels on connectome-wide association studies in
  fMRI. *NeuroImage*, *123*, 212–228.

Bellec, P., Marrelec, G., & Benali, H. (2008). A bootstrap test to investigate changes in brain
  connectivity for functional MRI. *Statistica Sinica*, *18*, 1253–1268.

Bellec, P., Rosa-neto, P., Lyttelton, O. C., Benali, H., & Evans, A. C. (2010). NeuroImage Multi-
  level bootstrap analysis of stable clusters in resting-state fMRI. *NeuroImage*, *51*(3), 1126–
  1139.

Bijsterbosch, J. D., Beckmann, C. F., Woolrich, M. W., Smith, S. M., & Harrison, S. J. (2019).
  The relationship between spatial configuration and functional connectivity of brain regions
  revisited. *eLife*, *8*. https://doi.org/10.7554/eLife.44890

Bijsterbosch, J. D., Woolrich, M. W., Glasser, M. F., Robinson, E. C., Beckmann, C. F., Van
  Essen, D. C., … Smith, S. M. (2018). The relationship between spatial configuration and
  functional connectivity of brain regions. *eLife*, Vol. 7. https://doi.org/10.7554/elife.32992

Blumensath, T., Jbabdi, S., Glasser, M. F., Van Essen, D. C., Ugurbil, K., Behrens, T. E. J., & Smith, S. M. (2013). Spatially constrained hierarchical parcellation of the brain with resting-state fMRI. *NeuroImage*, *76*, 313–324.

Boongoen, T., & Iam-On, N. (2018). Cluster ensembles: A survey of approaches with recent extensions and applications. *Computer Science Review*, *28*, 1–25.

Bosc, M., Heitz, F., Armspach, J. P., Namer, I., Gounot, D., & Rumbach, L. (2003). Automatic change detection in multimodal serial MRI: application to multiple sclerosis lesion evolution. *NeuroImage*, *20*(2), 643–656.

Breiman, L. (1996). Bagging predictors. *Machine Learning*, *24*(2), 123–140.

Breiman, L. (2001). Random Forests. *Machine Learning*, *45*(1), 5–32.

Bridgeford, E. W., Wang, S., Yang, Z., Wang, Z., Xu, T., Craddock, C., ... & Caffo, B. (2020). Big Data Reproducibility: Applications in Brain Imaging. *bioRxiv*, 802629.

Buckner, R. L., Krienen, F. M., Castellanos, A., Diaz, J. C., & Yeo, B. T. T. (2011). The organization of the human cerebellum estimated by intrinsic functional connectivity. *Journal of Neurophysiology*, *106*(July 2011), 2322–2345.

Chang, C., & Glover, G. H. (2010). Time-frequency dynamics of resting-state brain connectivity measured with fMRI. *NeuroImage*, *50*(1), 81–98.

Choi, E. Y., Yeo, B. T. T., & Buckner, R. L. (2012). The organization of the human striatum estimated by intrinsic functional connectivity. *Journal of Neurophysiology*, *108*(8), 2242–2263.

Cohen, A. L., Fair, D. A., Dosenbach, N. U. F., Miezin, F. M., Dierker, D., Van Essen, D. C., … Petersen, S. E. (2008). Defining functional areas in individual human brains using resting functional connectivity MRI. *NeuroImage*, *41*(1), 45–57.

Craddock, R. C., James, G. A., Holtzheimer, P. E., Hu, X. P., & Mayberg, H. S. (2012). A whole brain fMRI atlas generated via spatially constrained spectral clustering. *Human Brain Mapping*, *33*(8), 1914–1928.

Di Martino, A., O'Connor, D., Chen, B., Alaerts, K., Anderson, J. S., Assaf, M., … Milham, M. P. (2017). Enhancing studies of the connectome in autism using the autism brain imaging data exchange II. *Scientific Data*, *4*, 170010.

Di Martino, A., Yan, C.-G., Li, Q., Denio, E., Castellanos, F. X., Alaerts, K., … Milham, M. P. (2014). The autism brain imaging data exchange: towards a large-scale evaluation of the intrinsic brain architecture in autism. *Molecular Psychiatry*, *19*(6), 659–667.

Dinga, R., Schmaal, L., Penninx, B., van Tol, M. J., Veltman, D. J., van Velzen, L., … Marquand, A. (2018). Evaluating the evidence for biotypes of depression: attempted replication of Drysdale et.al. 2017 (p. 416321). https://doi.org/10.1101/416321

Dosenbach, N. U. F. N., Nardos, B., Cohen, A. L., Fair, D. a., Power, J. D., Church, J. a., … Schlaggar, B. L. (2010). Prediction of Individual Brain Maturity using fMRI. *Science*, *329*(5997), 1358–1361.

Drysdale, A. T., Grosenick, L., Downar, J., Dunlop, K., Mansouri, F., Meng, Y., … Liston, C. (2017). Resting-state connectivity biomarkers define neurophysiological subtypes of depression. *Nature Medicine*, *23*(1), 28–38.

Dudoit, S., & Fridlyand, J. (2003). Bagging to improve the accuracy of a clustering procedure. *Bioinformatics* , *19*(9), 1090–1099.

Dupré la Tour, T., Tallot, L., Grabot, L., Doyère, V., van Wassenhove, V., Grenier, Y., & Gramfort, A. (2017). Non-linear auto-regressive models for cross-frequency coupling in neural time series. *PLoS Computational Biology*, *13*(12), e1005893.

Efron, B., & Tibshirani, R. J. (1994). *An Introduction to the Bootstrap*. CRC Press.

Eickhoff, S. B., Yeo, B. T. T., & Genon, S. (2018). Imaging-based parcellations of the human brain. *Nature Reviews. Neuroscience*, *19*(11), 672–686.

Elliott, M. L., Knodt, A. R., Cooke, M., Kim, M. J., Melzer, T. R., Keenan, R., … Hariri, A. R. (2019). General functional connectivity: Shared features of resting-state and task fMRI drive reliable and heritable individual differences in functional brain networks. *NeuroImage*, *189*,

516–532.

Falk, E. B., Hyde, L. W., Mitchell, C., Faul, J., Gonzalez, R., Heitzeg, M. M., … Schulenberg, J. (2013). What is a representative brain? Neuroscience meets population science. *Proceedings of the National Academy of Sciences of the United States of America*, *110*(44), 17615–17622.

Finn, E. S., Shen, X., Scheinost, D., Rosenberg, M. D., Huang, J., Chun, M. M., … Finn, E. S. (2015). Functional connectome fingerprinting: identifying individuals using patterns of brain connectivity. *Nature Neuroscience*, *18*(October), 1–11.

Fischer, B., & Buhmann, J. M. (2003). Bagging for path-based clustering. *IEEE Transactions on Pattern Analysis and Machine Intelligence*, *25*(11), 1411–1415.

Fisher, A. J., Medaglia, J. D., & Jeronimus, B. F. (2018). Lack of group-to-individual generalizability is a threat to human subjects research. *Proceedings of the National Academy of Sciences of the United States of America*, *115*(27), E6106–E6115.

Fox, M. D., & Greicius, M. (2010). Clinical applications of resting state functional connectivity. *Frontiers in Systems Neuroscience*, *4*, 19.

Fred, A., & Lourenço, A. (2008). Cluster Ensemble Methods: from Single Clusterings to Combined Solutions. In O. Okun & G. Valentini (Eds.), *Supervised and Unsupervised Ensemble Methods and their Applications* (pp. 3–30). Berlin, Heidelberg: Springer Berlin Heidelberg.

Friedman, J., Hastie, T., & Tibshirani, R. (2001). *The elements of statistical learning* (Vol. 1). Springer series in statistics New York.

Garcia-Garcia, M., Nikolaidis, A., Bellec, P., Craddock, R. C., Cheung, B., Castellanos, F. X., & Milham, M. P. (2017). Detecting stable individual differences in the functional organization of the human basal ganglia. *NeuroImage*. https://doi.org/10.1016/j.neuroimage.2017.07.029

Glasser, M. F., Coalson, T. S., Robinson, E. C., Hacker, C. D., Harwell, J., Yacoub, E., … Van Essen, D. C. (2016). A multi-modal parcellation of human cerebral cortex. *Nature*,

536(7615), 171–178.

Gordon, E. M., Laumann, T. O., Adeyemo, B., Huckins, J. F., Kelley, W. M., & Petersen, S. E.
(2014). Generation and evaluation of a cortical area parcellation from resting-state
correlations. *Cerebral Cortex* , *26*(1), 288–303.

Gordon, E. M., Laumann, T. O., Adeyemo, B., & Petersen, S. E. (2015). Individual Variability of
the System-Level Organization of the Human Brain. *Cerebral Cortex* , bhv239.

Gordon, E. M., Laumann, T. O., Gilmore, A. W., Newbold, D. J., Greene, D. J., Berg, J. J., …
Dosenbach, N. U. F. (2017). Precision Functional Mapping of Individual Human Brains.
Neuron, *95*(4), 791–807.e7.

Gorgolewski, K., Burns, C. D., Madison, C., Clark, D., Halchenko, Y. O., Waskom, M. L., &
Ghosh, S. S. (2011). Nipype: A Flexible, Lightweight and Extensible Neuroimaging Data
Processing Framework in Python. *Frontiers in Neuroinformatics*, *5*.
https://doi.org/10.3389/fninf.2011.00013

Greene, D. J., Church, J. A., Dosenbach, N. U. F., Nielsen, A. N., Adeyemo, B., Nardos, B., …
Schlaggar, B. L. (2016). Multivariate pattern classification of pediatric Tourette syndrome
using functional connectivity MRI. *Developmental Science*, *19*(4), 581–598.

Hadjitodorov, S. T., Kuncheva, L. I., & Todorova, L. P. (2006). Moderate diversity for better
cluster ensembles. *An International Journal on Information Fusion*, *7*(3), 264–275.

Hagmann, P., Kurant, M., Gigandet, X., Thiran, P., Wedeen, V. J., Meuli, R., & Thiran, J.-P.
(2007). Mapping human whole-brain structural networks with diffusion MRI. *PloS One*, *2*(7),
e597.

Holmes, A. J., Hollinshead, M. O., O'Keefe, T. M., Petrov, V. I., Fariello, G. R., Wald, L. L., …
Buckner, R. L. (2015). Brain Genomics Superstruct Project initial data release with
structural, functional, and behavioral measures. *Scientific Data*, *2*, 150031.

Hong, S. J., Valk, S. L., Di Martino, A., Milham, M. P., & Bernhardt, B. C. (2018).
Multidimensional Neuroanatomical Subtyping of Autism Spectrum Disorder. *Cerebral*

Cortex, *28*(10), 3578–3588.

Hong, Y., Kwong, S., Wang, H., & Ren, Q. (2009). Resampling-based selective clustering ensembles. *Pattern Recognition Letters*, *30*(3), 298–305.

Hoyos-Idrobo, A., Schwartz, Y., Varoquaux, G., & Thirion, B. (2015). Improving sparse recovery on structured images with bagged clustering. *Pattern Recognition in NeuroImaging (PRNI), 2015 International Workshop on*, 73–76. IEEE.

Hutchison, R. M., Womelsdorf, T., Allen, E. A., Bandettini, P. A., Calhoun, V. D., Corbetta, M., … Chang, C. (2013). Dynamic functional connectivity: promise, issues, and interpretations. *NeuroImage*, *80*, 360–378.

Hu, X., & Yoo, I. (2004). Cluster Ensemble and Its Applications in Gene Expression Analysis. *Proceedings of the Second Conference on Asia-Pacific Bioinformatics - Volume 29*, 297–302. Darlinghurst, Australia, Australia: Australian Computer Society, Inc.

Janssen, R. J., Jylänki, P., Kessels, R. P. C., & van Gerven, M. A. J. (2015). Probabilistic model-based functional parcellation reveals a robust, fine-grained subdivision of the striatum. *NeuroImage*, *119*, 398–405.

JCGM. (2008). Evaluation of measurement data—Guide to the expression of uncertainty in measurement. *Int. Organ. Stand. Geneva ISBN*, *50*, 134.

Jernigan, T. L., Brown, T. T., Hagler, D. J., Jr, Akshoomoff, N., Bartsch, H., Newman, E., … Pediatric Imaging, Neurocognition and Genetics Study. (2016). The Pediatric Imaging, Neurocognition, and Genetics (PING) Data Repository. *NeuroImage*, *124*(Pt B), 1149–1154.

Jia, J., Xiao, X., Liu, B., & Jiao, L. (2011). Bagging-based spectral clustering ensemble selection. *Pattern Recognition Letters*, *32*(10), 1456–1467.

Johansen-Berg, H., Behrens, T. E. J., Sillery, E., Ciccarelli, O., Thompson, A. J., Smith, S. M., & Matthews, P. M. (2005). Functional–Anatomical Validation and Individual Variation of Diffusion Tractography-based Segmentation of the Human Thalamus. *Cerebral Cortex*,

15(1), 31–39.

Juang, L.-H., & Wu, M.-N. (2010). MRI brain lesion image detection based on color-converted K-means clustering segmentation. *Measurement*, *43*(7), 941–949.

Kelly, A. M. C., Di Martino, A., Uddin, L. Q., Shehzad, Z., Gee, D. G., Reiss, P. T., … Milham, M. P. (2009). Development of Anterior Cingulate Functional Connectivity from Late Childhood to Early Adulthood. *Cerebral Cortex* , *19*(3), 640–657.

Kelly, C., Toro, R., Di Martino, A., Cox, C. L., Bellec, P., Castellanos, F. X., & Milham, M. P. (2012). A convergent functional architecture of the insula emerges across imaging modalities. *NeuroImage*, *61*(4), 1129–1142.

Kim, D. J., Park, B., & Park, H. J. (2013). Functional connectivity-based identification of subdivisions of the basal ganglia and thalamus using multilevel independent component analysis of resting state fMRI. *Human brain mapping*, *34*(6), 1371-1385.

Kleinberg, J. M. (2003). An Impossibility Theorem for Clustering. In S. Becker, S. Thrun, & K. Obermayer (Eds.), *Advances in Neural Information Processing Systems 15* (pp. 463–470). MIT Press.

Klein, J. C., Behrens, T. E. J., Robson, M. D., Mackay, C. E., Higham, D. J., & Johansen-Berg, H. (2007). Connectivity-based parcellation of human cortex using diffusion MRI: Establishing reproducibility, validity and observer independence in BA 44/45 and SMA/pre-SMA. *NeuroImage*, *34*(1), 204–211.

Kong, R., Li, J., Orban, C., Sabuncu, M. R., Liu, H., Schaefer, A., … Yeo, B. T. T. (2019). Spatial Topography of Individual-Specific Cortical Networks Predicts Human Cognition, Personality, and Emotion. *Cerebral Cortex* , *29*(6), 2533–2551.

Krogh, A., & Vedelsby, J. (1995). Neural Network Ensembles, Cross Validation, and Active Learning. In G. Tesauro, D. S. Touretzky, & T. K. Leen (Eds.), *Advances in Neural Information Processing Systems 7* (pp. 231–238). MIT Press.

Kuncheva, L. I., & Hadjitodorov, S. T. (2004). Using diversity in cluster ensembles. *2004 IEEE*

International Conference on Systems, Man and Cybernetics (IEEE Cat. No.04CH37583), 2, 1214–1219 vol.2. ieeexplore.ieee.org.

Lambert, C., Simon, H., Colman, J., & Barrick, T. R. (2017). Defining thalamic nuclei and topographic connectivity gradients in vivo. *NeuroImage*, *158*, 466–479.

Lancichinetti, A., & Fortunato, S. (2012). Consensus clustering in complex networks. *Scientific Reports*, *2*, 336.

Lange, T., Roth, V., Braun, M. L., & Buhmann, J. M. (2004). Stability-based validation of clustering solutions. *Neural Computation*, *16*(6), 1299–1323.

Laumann, T. O., Gordon, E. M., Adeyemo, B., Snyder, A. Z., Joo, S. J., Chen, M.-Y., … Petersen, S. E. (2015). Functional System and Areal Organization of a Highly Sampled Individual Human Brain. *Neuron*, *87*(3), 657–670.

Liégeois, R., Laumann, T. O., Snyder, A. Z., Zhou, J., & Yeo, B. T. T. (2017). Interpreting temporal fluctuations in resting-state functional connectivity MRI. *NeuroImage*, *163*, 437–455.

Liem, F., Varoquaux, G., Kynast, J., Beyer, F., Kharabian Masouleh, S., Huntenburg, J. M., … Margulies, D. S. (2017). Predicting brain-age from multimodal imaging data captures cognitive impairment. *NeuroImage*, *148*, 179–188.

Li, H., Wu, G., Hu, X., Zhang, J., Li, L., & Wu, X. (2011). K-Means Clustering with Bagging and MapReduce. *2011 44th Hawaii International Conference on System Sciences*, 1–8. ieeexplore.ieee.org.

Li, T., & Ding, C. (2008). Weighted Consensus Clustering. In *Proceedings. Proceedings of the 2008 SIAM International Conference on Data Mining* (pp. 798–809). Society for Industrial and Applied Mathematics.

Margulies, D. S., Ghosh, S. S., Goulas, A., Falkiewicz, M., Huntenburg, J. M., Langs, G., … Smallwood, J. (2016). Situating the default-mode network along a principal gradient of macroscale cortical organization. *Proceedings of the National Academy of Sciences of the*

United States of America, *113*(44), 12574–12579.

Margulies, D. S., Kelly, A. M. C., Uddin, L. Q., Biswal, B. B., Castellanos, F. X., & Milham, M. P.

(2007). Mapping the functional connectivity of anterior cingulate cortex. *NeuroImage*, *37*(2),

579–588.

Mars, R. B., Jbabdi, S., Sallet, J., O'Reilly, J. X., Croxson, P. L., Olivier, E., … Rushworth, M. F.

S. (2011). Diffusion-Weighted Imaging Tractography-Based Parcellation of the Human

Parietal Cortex and Comparison with Human and Macaque Resting-State Functional

Connectivity. *Journal of Neuroscience*, Vol. 31, pp. 4087–4100.

https://doi.org/10.1523/jneurosci.5102-10.2011

Meinshausen, N., & Bühlmann, P. (2010). Stability selection. *Journal of the Royal Statistical*

Society. Retrieved from https://rss.onlinelibrary.wiley.com/doi/abs/10.1111/j.1467-

9868.2010.00740.x%4010.1111/%28ISSN%291467-9868.TOP_SERIES_B_RESEARCH

Meunier, D., Lambiotte, R., Fornito, A., Ersche, K. D., & Bullmore, E. T. (2009). Hierarchical

modularity in human brain functional networks. *Frontiers in Neuroinformatics*, *3*, 37.

Millman, K. J., Brett, M., Barnowski, R., & Poline, J.-B. (2018). Teaching Computational

Reproducibility for Neuroimaging. *Frontiers in Neuroscience*, *12*, 727.

Myers, P. E., Arvapalli, G. C., Ramachandran, S. C., Pisner, D. A., Frank, P. F., Lemmer, A. D.,

… Vogelstein, J. T. (2019). Standardizing Human Brain Parcellations (p. 845065).

https://doi.org/10.1101/845065

Nelson, S. M., Cohen, A. L., Power, J. D., Wig, G. S., Miezin, F. M., Wheeler, M. E., …

Petersen, S. E. (2010). A parcellation scheme for human left lateral parietal cortex. *Neuron*,

67(1), 156–170.

Nichols, T. E., Das, S., Eickhoff, S. B., Evans, A. C., Glatard, T., Hanke, M., … Yeo, B. T. T.

(2017). Best practices in data analysis and sharing in neuroimaging using MRI. *Nature*

Neuroscience, *20*(3), 299–303.

Nikolaidis, A., Goatz, D., & Smaragdis, P. (2015). Predicting Skill-Based Task Performance and

Learning with fMRI Motor and Subcortical Network Connectivity. *Pattern Recognition in*.

Retrieved from https://ieeexplore.ieee.org/abstract/document/7270856/

Nikolaidis, A., Voss, M. W., Lee, H., Vo, L. T. K., & Kramer, A. F. (2014). Parietal plasticity after training with a complex video game is associated with individual differences in improvements in an untrained working memory task. *Frontiers in Human Neuroscience*, *8*, 169.

Noble, S., Spann, M. N., Tokoglu, F., Shen, X., Constable, R. T., & Scheinost, D. (2017). Influences on the Test–Retest Reliability of Functional Connectivity MRI and its Relationship with Behavioral Utility. *Cerebral Cortex* , *27*(11), 5415–5429.

O'Connor, D., Potler, N. V., Kovacs, M., Xu, T., Ai, L., Pellman, J., … Milham, M. P. (2017). The Healthy Brain Network Serial Scanning Initiative: a resource for evaluating inter-individual differences and their reliabilities across scan conditions and sessions. *GigaScience*, *6*(2), 1–14.

Oelhafen, S., Nikolaidis, A., Padovani, T., Blaser, D., Koenig, T., & Perrig, W. J. W. J. (2013). Increased parietal activity after training of interference control. *Neuropsychologia*, *51*(13), 2781–2790.

Pedregosa, F., Varoquaux, G., Gramfort, A., Michel, V., Thirion, B., Grisel, O., … Duchesnay, É. (2011). Scikit-learn: Machine Learning in Python. *Journal of Machine Learning Research: JMLR*, *12*(Oct), 2825–2830.

Power, J. D., Barnes, K. A., Snyder, A. Z., Schlaggar, B. L., & Petersen, S. E. (2012). Spurious but systematic correlations in functional connectivity MRI networks arise from subject motion. *NeuroImage*, *59*(3), 2142–2154.

Priebe, C. E., Park, Y., Vogelstein, J. T., Conroy, J. M., Lyzinski, V., Tang, M., … Bridgeford, E. (2019). On a two-truths phenomenon in spectral graph clustering. *Proceedings of the National Academy of Sciences of the United States of America*, *116*(13), 5995–6000.

Salehi, M., Greene, A. S., Karbasi, A., Shen, X., Scheinost, D., & Constable, R. T. (2020). There

is no single functional atlas even for a single individual: Functional parcel definitions

change with task. *NeuroImage*, *208*, 116366.

Schaefer, A., Kong, R., & Yeo, B. T. T. (2016). Chapter 1 - Functional connectivity parcellation

of the human brain. In G. Wu, D. Shen, & M. R. Sabuncu (Eds.), *Machine Learning and*

Medical Imaging (pp. 3–29). Academic Press.

Shehzad, Z., Kelly, C., Reiss, P. T., Cameron Craddock, R., Emerson, J. W., McMahon, K., …

Milham, M. P. (2014). A multivariate distance-based analytic framework for connectome-

wide association studies. *NeuroImage*, *93*(October 2015), 74–94.

Shen, X., Tokoglu, F., Papademetris, X., & Constable, R. T. (2013). Groupwise whole-brain

parcellation from resting-state fMRI data for network node identification. *NeuroImage*, *82*,

403–415.

Shrout, P. E., & Fleiss, J. L. (1979). Intraclass correlations-uses in assessing rater reliability.

Psychological Bulletin, *86*(2), 420–428.

Strehl, A., & Ghosh, J. (2002). Cluster Ensembles --- A Knowledge Reuse Framework for

Combining Multiple Partitions. *Journal of Machine Learning Research: JMLR*, *3*(Dec), 583–

617.

Talukdar, T., Nikolaidis, A., Zwilling, C. E., Paul, E. J., Hillman, C. H., Cohen, N. J., … Barbey,

A. K. (2017). Aerobic Fitness Explains Individual Differences in the Functional Brain

Connectome of Healthy Young Adults. *Cerebral Cortex* , 1–10.

Thirion, B., Varoquaux, G., Dohmatob, E., & Poline, J. B. (2014). Which fMRI clustering gives

good brain parcellations? *Frontiers in Neuroscience*, *8*(8 JUL), 1–13.

Tumer, K., & Ghosh, J. (1999). Linear and order statistics combiners for pattern classification.

CoRR. *arXiv Preprint Cs. NE/9905012*. Retrieved from http://arxiv.org/abs/cs.NE/9905012

van den Heuvel, M., Mandl, R., & Pol, H. H. (2008). Normalized cut group clustering of resting-

state fMRI data. *PloS One*, *3*(4). https://doi.org/10.1371/journal.pone.0002001

Varoquaux, G., Gramfort, A., Pedregosa, F., Michel, V., & Thirion, B. (2011). Multi-subject

dictionary learning to segment an atlas of brain spontaneous activity. *Information*

Processing in Medical Imaging: Proceedings of the ... Conference, *22*, 562–573.

Volkow, N. D., Koob, G. F., Croyle, R. T., Bianchi, D. W., Gordon, J. A., Koroshetz, W. J., …

Weiss, S. R. B. (2018). The conception of the ABCD study: From substance use to a broad

NIH collaboration. *Developmental Cognitive Neuroscience*, *32*, 4–7.

von Luxburg, U. (2010). Clustering Stability: An Overview. *Foundations and Trends® in Machine*

Learning, *2*(3), 235–274.

Wig, G. S., Laumann, T. O., Cohen, A. L., Power, J. D., Nelson, S. M., Glasser, M. F., …

Petersen, S. E. (2014). Parcellating an individual subject's cortical and subcortical brain

structures using snowball sampling of resting-state correlations. *Cerebral Cortex* , *24*(8),

2036–2054.

Xu, T., Opitz, A., Craddock, R. C., Wright, M. J., Zuo, X.-N., & Milham, M. P. (2016). Assessing

Variations in Areal Organization for the Intrinsic Brain: From Fingerprints to Reliability.

Cerebral Cortex , *26*(11), 4192–4211.

Yan, C.-G., Cheung, B., Kelly, C., Colcombe, S., Craddock, R. C., Di Martino, A., … Milham, M.

P. (2013). A comprehensive assessment of regional variation in the impact of head

micromovements on functional connectomics. *NeuroImage*, *76*, 183–201.

Yeo, B. T. T., Krienen, F. M., Sepulcre, J., Sabuncu, M. R., Lashkari, D., Hollinshead, M., …

Buckner, R. L. (2011). *The organization of the human cerebral cortex estimated by intrinsic*

functional connectivity. 1125–1165.

Zalesky, A., Fornito, A., Harding, I. H., Cocchi, L., Yücel, M., Pantelis, C., & Bullmore, E. T.

(2010). Whole-brain anatomical networks: does the choice of nodes matter? *NeuroImage*,

50(3), 970–983.

Zhou, Z.-H. (2012). *Ensemble Methods: Foundations and Algorithms*. CRC Press.

Zuo, X.-N., Anderson, J. S., Bellec, P., Birn, R. M., Biswal, B. B., Blautzik, J., … Milham, M. P.

(2014). An open science resource for establishing reliability and reproducibility in functional

connectomics. *Scientific Data*, *1*, 140049.

Zuo, X.-N., Kelly, C., Di Martino, A., Mennes, M., Margulies, D. S., Bangaru, S., … Milham, M.

P. (2010). Growing together and growing apart: regional and sex differences in the lifespan

developmental trajectories of functional homotopy. *The Journal of Neuroscience: The*

Official Journal of the Society for Neuroscience, *30*(45), 15034–15043.

Zuo, X.-N., & Xing, X.-X. (2014). Test-retest reliabilities of resting-state FMRI measurements in

human brain functional connectomics: a systems neuroscience perspective. *Neuroscience*

and Biobehavioral Reviews, *45*, 100–118.

Zuo, X.-N., Xu, T., & Milham, M. P. (2019). Harnessing reliability for neuroscience research.

Nature Human Behaviour. https://doi.org/10.1038/s41562-019-0655-x

5. Supplementary Materials.

5.1 Supplementary Methods

5.1.1 Standard Clustering Resampling Datasets- Without bagging, Ward's criterion hierarchical agglomerative cluster is deterministic and has no variance over multiple runs. To offer a better understanding of the sampling variance that could lead to differences in clustering when bagging is not applied, we apply resampling to the original replication datasets when comparing them to a given reference. To create the multiple 3- and 5-minute datasets for the non-bootstrapped condition, we randomly sampled continuous 3- or 5-minute blocks of the full 50 minute replication dataset. To create the 10, 15, 20, 25, and 50-minute resampled datasets, we randomly sampled continuous 5-minute blocks of the full 50-minute replication dataset. We did not calculate resampling in the GSP datasets because we compared the 10 groups against one another.

5.1.2 PyBASC- Originally, this method was implemented in Octave, and we have recently implemented this method in Python to take advantage of the broad range of powerful libraries available for machine learning and neuroimaging, including NiBabel, Nilearn, Scikit Learn, and NiPype. This enables PyBASC to be highly flexible and extensible in adopting new clustering algorithms and implementations, but more importantly allows for dramatic increases in computational power through the use of NiPype's easy-to-use and adjust multi-core processing capabilities. We have also made edits to the processing that make PyBASC run very efficiently with minimal memory loads. This makes PyBASC just as easy to run on a laptop as on a large server in the cloud. Here, we briefly address the PyBASC overall methodology. For more information, we have also explained these methods in more detail elsewhere (Bellec et al., 2010; Garcia-Garcia et al., 2017). PyBASC has a wide range of functionalities that can be customized according to user preferences. Well-performing default values are provided where applicable, but users can choose 1) the number of initial supervoxels, 2) the number of individual and 3) group-

level bootstraps, the 4) region to be parcellated and 5) the secondary region (optional) to use as

the basis of cross- network clustering. Users can also define the cluster method to be used, as

well as the affinity threshold and distance metric used in the clustering procedures.

5.1.3 Individual-Level- First to reduce the dimensionality of the voxel wise time series, and to allow

for better computational efficiency, we apply a hierarchical feature agglomeration from Scikit

Learn with a neighboring voxel spatial constraint to each individual's data (Subcortical

Parcellation: 600 supervoxels; Cortical Parcellation: 1800 supervoxels). Then, a circular block

bootstrap procedure is applied to create resampled time series data from the original functional

image. We follow prior recommendations to set the block length to greater than 20 time steps

(Adolf et al., 2014), and more specifically, equal to the square root of the number of points in a

time series (Bellec et al., 2010; Bellec et al., 2008). Each of these resampled time series are then

clustered using the clustering technique of choice. Currently K-means, Ward's criterion

hierarchical agglomerative, spectral clustering, and Gaussian mixture models are implemented.

With each application of clustering, the cluster labels are transformed into an adjacency matrix of

0s and 1s representing whether a given voxel belongs to the same cluster as another voxel. Each

of these adjacency matrices are in supervoxel space, which differs between individuals.

Therefore, the dimension reduction procedure is reversed to create a voxel wise adjacency matrix

that puts all individual level data back into the same space. All adjacency matrices are averaged

together to create an individual mean adjacency matrix (IMA), which represents a summary of all

clustering assignments across all bootstraps. The IMA can be clustered to produce a final

consensus cluster assignment for each individual, and it can be used in group level bagging.

5.1.4 Group Level- PyBASC applies bagging to IMAs across individuals, recreating resampled

groups of IMAs from the original pool of participants. The IMAs for each group level bootstrap are

averaged and another group adjacency matrix is created through clustering. The adjacency matrix

across all bootstraps are averaged to create a group mean adjacency matrix (GMA), and this GMA is clustered to create the final group level clustering. The GMA is the final output of the group level bagging, along with the cluster labels. While the IMA represents a summary of the clustering across all bootstraps for each individual, the GMA represents a summary of the clustering across all bootstraps for the group. We compare each individual's IMA to the GMA as a detailed way of assessing similarities between the individual and group level clustering.

5.2 Supplementary Results

5.2.1- Here we compare the voxelwise cluster assignment differences between the Reference GSP dataset created with 400 bootstraps and the 10- and 50-minute HNU1 parcellations. Bright blue corresponds to all comparisons being different between the two parcellations across all replication samples with 400 bootstraps, and dark purple shows where there are no differences between parcellations. We find that both 10- and 50-minute parcellations mostly differ from the GSP in transition zones between parcels. In particular we see these difference maps reveal a superior-inferior thalamic transition zone, and a putamen-pallidum transition zone. Notably, the HNU1 50-minute parcellation differs from the GSP reference in differential classification of the caudate. Whereas the 50-minute HNU1 data clusters the bilateral caudate into the same cluster, both the GSP and the 10-minute HNU1 data cluster the caudate into separate, non-homologous clusters.

HNU Repeatability Difference Maps

10 min   50 min

5.2.2- Here we compare differences the HNU1 Replication and Reference parcellations. Bright yellow corresponds to all comparisons being different between the two parcellations across all replication samples with 400 bootstraps, and dark purple shows where there are no differences between parcellations. Notably we see differentiation between reference and the 10-minute parcellation is higher than the 50-minute replication set. Furthermore, we see a reprise of the transition zones seen in S1, notably a clear superior-inferior transition, and a putamen-pallidum transition as well.

5.2.3- Univariate Reliability in GSP with motion regressed out. Motion can be a source of highly
reproducible signal in MRI data. We wanted to make sure the impact of bagging wasn't being
driven by motion, and so we regressed out motion from each individual mean adjacency matrix
before calculating ICC. As was the case without motion regression, here we see that bagging
improves the ICC of parcellations. A,B,C show the top 50%, 75%, and 95% ICC values for the
individual level mean adjacency matrices. Each point corresponds to the 50th, 75th, and 95th
percentile ICC values for the individual level mean adjacency matrices for each of the 10 GSP
groups. D and E show the mean squared error within individuals and between individuals
respectively. We see that bagging improves ICC, it has a dramatic impact on both MSE and
MSR, with samples with the lowest drop in MSR showing the greatest pickup in ICC.

5.2.4 - Bagging improvements generalize across spatial constraints. This figure demonstrates
bagging improves between session reproducibility in subcortical parcellation across levels of
spatial constraints. In the 'Low' spatial constraint condition, the approximately 1800 voxels of the
subcortical region of interest are reduced slightly to 600 supervoxels separately for each
individual. In the "Full" spatial constraint condition, the subcortical parcels are fully spatially
constrained, meaning that no discontiguous parcels exist. We find that bagging improves
reproducibility of the parcellations in both these conditions.

2   5.2.5 Bagging Improves between session reproducibility of subcortical parcellation with spectral
3   clustering. This figure demonstrates that the beneficial impact of bagging generalizes across
4   clustering techniques as well. Notably however, while the spatial correlation of the parcellation
5   improves considerably with bagging for both 20- and 50-minute scans, ARI only shows significant
6   improvements for 50 minutes of data.