Modeling second-order boundary perception: A machine learning approach

Abbreviated Title: Modeling second-order boundary perception

Christopher DiMattina [1,*] and Curtis L. Baker, Jr.[2]

[1]Computational Perception Laboratory, Department of Psychology,
Florida Gulf Coast University, Fort Myers, FL, USA 33965-6565

[2]McGill Vision Research Unit, Department of Ophthalmology,
McGill University, Montreal, QC, Canada H3G1A4

*Corresponding Author:
        Christopher DiMattina
        Whitaker Hall Room 215
        Florida Gulf Coast University
        10501 FGCU Blvd S.
        Fort Myers, FL 33965-6565

        Email: cdimattina@fgcu.edu
        Web: http://itech.fgcu.edu/faculty/cdimattina/
        Tel: (239)-590-1513

Conflict of Interest: The authors declare no competing financial interests.

Acknowledgements: We thank the FGCU undergraduates in the Computational Perception Lab for help with data collection, Wilson S. Geisler for code implementing decision-variable correlation, Elizabeth Zavitz for micropattern texture stimuli, and Fred Kingdom for helpful discussions and comments. Supported by Canadian NSERC Grants OPG0001978 and RGPIN-2017-05292 to C.L.B. and a FGCU Professional Development Grant to C.D.

Abstract

Background: Visual pattern detection and discrimination are essential first steps for scene analysis. Numerous human psychophysical studies have modeled visual pattern detection and discrimination by estimating linear templates for classifying noisy stimuli defined by spatial variations in pixel intensities. However, such methods are poorly suited to understanding sensory processing mechanisms for complex visual stimuli such as second-order boundaries defined by spatial differences in contrast or texture.

Methodology / Principal Findings: We introduce a novel machine learning framework for modeling human perception of second-order visual stimuli, using image-computable hierarchical neural network models fit directly to psychophysical trial data. This framework is applied to modeling visual processing of boundaries defined by differences in the contrast of a carrier texture pattern, in two different psychophysical tasks: (1) boundary orientation identification, and (2) fine orientation discrimination. Cross-validation analysis is employed to optimize model hyper-parameters, and demonstrate that these models are able to accurately predict human performance on novel stimulus sets not used for fitting model parameters. We find that, like the ideal observer, human observers take a region-based approach to the orientation identification task, while taking an edge-based approach to the fine orientation discrimination task. How observers integrate contrast modulation across orientation channels is investigated by fitting psychophysical data with two models representing competing hypotheses, revealing a preference for a model which combines multiple orientations at the earliest possible stage. Our results suggest that this machine learning approach has much potential to advance the study of second-order visual processing, and we outline future steps towards generalizing the method to modeling visual segmentation of natural texture boundaries.

Conclusions / Significance: This study demonstrates how machine learning methodology can be fruitfully applied to psychophysical studies of second-order visual processing.

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Many naturally occurring visual boundaries are defined by spatial differences in features other

than luminance, for example by differences in texture or contrast. Quantitative models of such

"second-order" boundary perception cannot be estimated using the standard regression

techniques (known as "classification images") commonly applied to "first-order", luminance-

defined stimuli. Here we present a novel machine learning approach to modeling second-order

boundary perception using hierarchical neural networks. In contrast to previous quantitative

studies of second-order boundary perception, we directly estimate network model parameters

using psychophysical trial data. We demonstrate that our method can reveal different spatial

summation strategies that human observers utilize for different kinds of second-order boundary

perception tasks, and can be used to compare competing hypotheses of how contrast modulation

is integrated across orientation channels. We outline extensions of the methodology to other

kinds of second-order boundaries, including those in natural images.

Introduction

Many of the most common functions of sensory systems involve detection, identification or discrimination of particular stimuli. For example, a critically important ability of early visual processing is to segment images into distinct regions, which may correspond to cohesive surfaces or objects (Marr, 1982). To better understand the underlying mechanisms, it would be useful to fit biologically plausible models of surface segmentation to psychophysical data, and assess how well such models can account for independent datasets.

A widely used approach to modeling human psychophysics has been to assume that performance can be understood in terms of how well a visual stimulus matches an internal "template", typically modeled as a linear spatial filter. This approach uses high-dimensional regression models fit to data from tasks in which a subject detects or classifies a sensory stimulus presented with superimposed white noise (Ahumada, 1996, 2002; Neri & Levi, 2006; Murray, 2011), to recover an estimate of the linear filter that best accounts for the data. This system-identification (SI) approach to psychophysics, often called "psychophysical reverse correlation" or "classification image analysis", parallels neurophysiology studies that fit linear filter models to neural responses elicited by white noise stimuli (e.g. DeAngelis, Ohzawa, & Freeman 1993; Chichilnisky, 2001). Psychophysical SI methods have been applied in varied problem domains and yielded valuable insight into perceptual mechanisms (Abbey & Eckstein, 2002; Eckstein, Shimozaki, & Abbey, 2002; Li, Levi, & Klein, 2004; Neri & Levi, 2006; Morgenstern & Elder, 2012; McIlhagga & May, 2012; Kurki, Saarinen, & Hyvarinen, 2014).

One limitation of most previous psychophysical system identification studies has been the use of stimuli that are typically defined by spatial or temporal variations in first-order statistics like luminance or color. However, many natural visual stimuli such as occlusion boundaries (Fig. 1a, top) are defined by spatial variations in higher-order image statistics, e.g. texture or contrast, rather than simple luminance differences (Schofield, 1999; Konishi et al., 2003; Johnson & Baker, 2004; Martin, Fowlkes, & Malik, 2004; DiMattina, Fox, & Lewicki, 2012). Such "second-order" boundaries (Fig. 1a, bottom) have been of particular interest because their detection cannot be explained by simple linear filters (Baker, 1999; Landy & Graham, 2004), and consequently human performance cannot be readily modeled using

conventional psychophysical SI methods. More generally, there is a need for a psychophysical

modeling approach that can handle a broader range of stimuli and tasks.

Here we present a novel machine learning method to extend psychophysical SI to more

complex naturalistic stimuli such as second-order boundaries. Our general approach is to fit

image-computable hierarchical neural network models of second-order vision (Fig. 2) directly to

psychophysical trial data, similar to recent studies using multi-stage models to characterize

nonlinear responses in sensory neurons (Willmore, Prenger, & Gallant, 2010; Vintch, Movshon,

& Simoncelli, 2015; Harper et al. 2016; Rowenkamp & Sharpee, 2017). Our application of this

framework generalizes a class of biologically plausible "Filter-Rectify-Filter" (FRF) models that

have often been invoked to explan second-order processing (Landy & Graham, 2004). However,

in contrast to previous general schemes for second-order vision (e.g. Malik & Perona, 1990;

Bergen & Landy, 1991; Graham, Beck & Sutter, 1992) and quantitative models (Zavitz & Baker,

2013; Westrick & Landy, 2013), we take a machine learning approach in which we estimate the

defining model parameters by direct fitting to psychophysical trial data. This permits more

incisive tests of predictions on novel datasets in order to validate our models, and to evaluate

competing models.

We focus on contrast-defined second-order boundaries (Fig. 1a, b) since they are well

studied psychophysically (Dakin & Mareschal, 2000; Schofield & Georgeson, 1999, 2003;

Ledgeway & Smith, 1994; Ellemberg, Allen, & Hess 2006), and there are neurons in the early

mammalian visual cortex that give selective responses to contrast modulation stimuli (Mareschal

& Baker, 1998; Tanaka & Ohzawa, 2009; Rosenberg et al, 2010; Li et al., 2014). We model

performance on two tasks making use of contrast-defined boundaries: (1) identification of

boundary orientation, and (2) boundary orientation discrimination (Fig. 1c). We find that

subjects utilize spatial information in markedly different ways for these two tasks, employing

"region-based" processing for the orientation identification task and "edge-based" processing for

the orientation discrimination task, in both cases consistent with an ideal observer.

We further demonstrate the power of this methodology for evaluating competing

hypotheses regarding the nature of channel summation within the FRF scheme (Kingdom, Prins,

& Hayes, 2003; Motoyoshi & Nishida, 2004; Motoyoshi & Kingdom, 2007; Westrick & Landy

2013) by comparing the ability of two different model architectures to fit human performance on

a contrast edge detection task in which the carrier pattern contains elements with two

orientations. Post-hoc Bayesian model comparison (Schwarz, 1978; Kass & Raferty, 1995;

Bishop, 2006) demonstrates a preference for a model in which carrier pattern orientation is

integrated across channels by the second-stage filters, consistent with previous psychophysical

studies (e.g., Motoyoshi & Nishida, 2004).

Finally, we discuss potential applications of this methodology to future quantitative

studies of first- and second-order cue integration (Allard & Faubert, 2007; Saarela & Landy,

2012; Hutchinson, Ledgeway, & Baker, 2016) and natural boundary detection (McDermott,

2004; DiMattina et al., 2012). We suggest that the application of machine learning methodology

similar to that presented here can potentially help to better quantify visual processing of natural

occlusion boundaries and complex natural visual stimuli more generally.

Results

Observers performed two different psychophysical tasks making use of contrast-modulated

boundary stimuli like those shown in Fig. 1 (see Methods). In the first task, orientation-

identification (Fig. 1c, left), observers determined in which of two oblique orientations (-/+ 45

deg, L/R) a near-threshold contrast boundary was presented, with varying amounts of contrast

modulation (Experiments 1 and 3). We also employed an orientation-discrimination task (Fig.

1c, right) in which observers indicated the orientation (L/R) of a supra-threshold contrast

boundary, whose orientation was perturbed slightly from vertical by varying amounts (-/+ 6-7

deg.) (Experiment 2). Trial-wise responses obtained from these experiments were used to fit and

evaluate a model (Fig. 2) implementing a "Filter-Rectifty-Filter" (FRF) operation (Landy &

Graham, 2004) on each stimulus image, with the goal of characterizing the nature of spatial

summation for perception of contrast boundaries, as well as the shape of the second-stage filter

nonlinearity. We describe the model in greater depth before presenting the experimental results.

Modeling framework

The model used to fit psychophysical trial data (Fig. 2) employed a first stage comprised of a

bank of fine-scale Gabor filters that compute local oriented energy in a manner similar to V1

complex cells (Adelson & Bergen, 1985). The second stage consisted of a pair of filters,

representing the two task alternatives (L/R), each instantiated by a weighted sum of the

normalized outputs of the first-stage filters. In contrast to the first-stage filters, these second-

stage filters analyze the image at a more coarse spatial scale, integrating variations in contrast

across the boundary. Finally, the outputs of these two second-stage filters are passed through a

static non-linearity $h(u) = |u|^\alpha$ and then compared to decide on a trial-by-trial basis if a given

stimulus boundary appeared more likely to be tilted left or right (L/R), i.e. the probability $0 <$

$P(R) < 1$ of the stimulus being classified by the observer as R. The main goal of Experiments 1

and 2 was to estimate the shapes of the second-stage filters.

To reduce model parameter space dimensionality, we performed downsampling between

the first- and second-stage filters, i.e. pooling of spatially adjacent first-stage filter responses.

Here we implemented three alternative methods: (1) simple averaging (AVG), (2) maximum

(MAX) (Goodfellow, Bengio, & Courville, 2016), and (3) sub-sampling (SUB) (Bergen &

Landy, 1991). In Experiment 1 we considered all three pooling rules; most analyses utilized

16x16 downsampling, but 3 downsampling sizes (22x22, 16x16 and 8x8) were compared. In

Experiments 2 and 3 we considered only AVG pooling and a single downsampling size

(Experiment 2: 22x22, Experiment 3: 12x12).

We implement the model's final (L/R) classification in two alternative ways: In the

deterministic model (DET), if the output of the L filter is larger than that of the R filter (plus the

bias term) so that $P(R) > 0.5$, the stimulus will be classified as R, otherwise it is classified as L.

In the *stochastic* model (STO), the output $P(R)$ specifies only the probability of classifying the

stimulus as R or L, thus introducing randomness to the model without requiring an additional

free parameter.

A common approach to make the estimation problem more tractable is to utilize

reasonable prior constraints on the model parameter space (Mineault, Barthelme, & Pack, 2009;

Wu, David & Gallant, 2006; Park & Pillow, 2011). Here we use two kinds of Bayesian priors:

(1) ridge-regression (Hoerl & Kennard, 1970; Bishop 2006) to penalize large weights (*ridge*),

and (2) ridge-regression combined with an additional smoothness prior (Mineault et al., 2009) to

penalize excessively "rough" second-stage filter weight profiles (*ridge + smooth*). Additional

details of the model are given in Methods.

Experiment 1: Boundary orientation identification

<u>Stimuli and task</u>

Observers viewed contrast-defined texture boundaries with varying degrees of modulation depth

(Fig. 1b), and performed forced-choice judgments of whether the boundary was oriented right- or

left-oblique (45 degrees clockwise or counterclockwise, Fig.1c left). In Experiment 1-VAR (7

observers), a method of constant stimuli was used to vary contrast modulation depth over a range

spanning values near threshold but also including some levels producing near-perfect, or chance,

performance. In another version (Experiment 1-FIX, 3 observers) the contrast modulation depth

was held constant at a near-threshold level.

Model fit to representative observers

Fig. 3a shows the results of fitting the model (16x16 downsampling, AVG pooling) to data from

one representative observer (AMA) in Experiment 1-VAR. The top panels show estimated

second-stage filter weights as image maps across the spatial extent of the stimuli, with pixel

color indicating weight values. The black dashed lines in the bottom plots show mean 1-D

profiles, obtained by collapsing the 2-D weight maps orthogonally to the boundary orientations,

whereas thick solid lines (red = *ridge*, green = *ridge + smooth*) show profiles obtained from over

30 bootstrap-resampled training sets. We see that these mean 1-D profiles are nearly

indistinguishable from one another, all resembling a step-like function (see below). While many

of the individual 2-D weights can be quite variable (Supplementary Fig. S7), the 1-D weight

profile magnitudes lie well above zero (Fig. 3, thin dashed lines show +/- 1 SEM). The addition

of the smoothing prior (*ridge + smooth*) results in weighting functions that are very similar, but

less "noisy" in appearance, consistent with previous results with classification images and

receptive field modeling (Mineault et al., 2009; Park and Pillow, 2011). Furthermore, all three

pooling rules (AVG, MAX, SUB) yielded consistent 2-D and 1-D weight profiles

(Supplementary Fig. S8).

Fig. 3b shows the model fit to data from a representative observer (JJF) in Experiment 1-

FIX. In this version of the experiment, the contrast modulation depth was kept constant at

approximately threshold level for each observer (Supplementary Table S1), similar to most

previous work in the classification image literature (Abbey & Eckstein, 2002; Murray, 2011).

Here we see very similar results as for the observer in Experiment 1-VAR, also showing a step-

like function for this task. As before, this result was robust to the pooling rule (Supplementary

Fig. S9).

To assess the extent to which observers were employing the same spatial integration as an

ideal observer, we fit the model to stimulus category labels rather than observer responses. The

2-D weight maps and 1-D profiles obtained for an ideal observer in Experiment 1-VAR (Fig. 3c),

reveal that the ideal weight map is a step-like function like that seen in the human results. Similar

results for an ideal observer fit to stimulus category labels in Experiment 1-FIX are shown in

Supplementary Fig. S10.

<u>Edge-based vs. region-based analysis</u>

When finding a boundary between adjacent textures, the visual system might make use only of

texture elements close to the boundary ("edge-based"), or it might utilize the entirety of both

adjacent texture regions ("region-based"). A number of previous studies have investigated this

question for textures defined by orientation differences (Nothdurft, 1985; Gurnsey & Laundry,

1992; Wolfson & Landy, 1998), but to the best of our knowledge this issue has not been

addressed systematically for contrast-defined textures. The results from two individual observers

(Fig. 3a) as well as an ideal observer (Fig. 3b) indicate that the entire texture regions on either

side of the boundary are contributing to performance, giving step-like 1-D profiles - all

indicative of "region-based" processing.

To examine the robustness of this result across observers and for different model variants,

Fig. 4 shows the 1-D averaged profiles of second-stage filter weights for all observers (thin

colored lines) and group averages (thick black lines) in Experiment 1-VAR (Fig. 4a) and

Experiment 1-FIX (Fig. 4b). We see that the magnitudes of the 1-D weights are approximately

constant as one moves from the diagonal to the boundary, indicative of region-based processing,

and that these results are also consistent for all three pooling rules (AVG, MAX, SUB). To

explore whether the step-like 1-D profile result is consistent with an ideal observer, plots of the

normalized (scaled to unit norm) ideal observer 1-D weight profiles (30 bootstraps) are shown in

Fig. 5a as thick black lines, with 95% confidence intervals (+/- 1.96 SEM) plotted as dashed

black lines. We see that the normalized 1-D weight profiles for individual observers (dashed

color lines), and for means over observers (thick red dashed lines) generally lie within the 95%

confidence intervals of the ideal observer. Therefore, the performance of the human observers is

very much consistent with that of the ideal observer, both of which give similar step-like profiles

and thus seem to integrate contrast information across the whole region.

To test whether our finding of region-based processing was robust to increasing the

carrier spatial frequency, we ran an additional control version of the experiment on 3 naïve

observers (Experiment 1-HFC) in which we reduced the micropattern size from 32 to 8 pixels

(while increasing the density by a factor of 4). Such a stimulus would potentially engage many

more contrast-modulation tuned neurons having receptive fields localized to the boundary (Li et

al., 2014), potentially revealing edge-based processing. However, even with the high-frequency

carrier we still observed region-based processing (Fig. 5b), consistent with an ideal observer.

Second-stage filter nonlinearity

In Experiment 1, the best-fit expansive nonlinearity exponent α for the second-stage filters is

greater than unity for all observers, for both the *ridge* and *ridge + smooth* priors. For Experiment

1-VAR with AVG sampling, median α values were around 2 (*ridge*: median = 2.15, min = 1.70,

max = 2.85; *ridge + smooth*: median = 1.95, min = 1.70, max = 3.35, N = 7), and for Experiment

1-FIX we obtained median values closer to 1.5 (*ridge*: median = 1.50, min = 1.40, max = 1.60;

ridge + smooth: median = 1.60, min = 1.60, max = 1.90, N = 3). Similar results were obtained

for other downsampling methods (Supplementary Tables S2, S3), and the ideal observer was also

best fit with an expansive nonlinearity (AVG; Experiment 1-VAR: *ridge*: 4.00; *ridge + smooth*:

3.30; Experiment 1-FIX: *ridge*: 2.20; *ridge + smooth*: 2.30). Plots of the second-stage

nonlinearities for observers AMA, JJF are shown in Supplementary Fig. S11. This finding is

consistent with previous studies suggesting an accelerating nonlinearity following the second-

stage filters (see Discussion).

Analysis of model accuracy

To better assess the meaningfulness of the above model-fitting results, it is important to make

quantitative measures of the fitted models' accuracy in predicting observers' responses to novel

stimuli. Such measures can also address the relative merit of different variants of the estimation

procedure (*ridge* vs *ridge+smooth* prior) and of the model details, such as downsampling method

(AVG, MAX, SUB) and classification rule (DET, STO). In this section we describe some of our

analyses of model performance, and refer to other assessments in the Supplementary Material.

Psychometric function agreement

To the extent that the model architecture is appropriate and the data are sufficient to obtain

accurate estimates of parameters, then the fitted model should be able to predict each observer's

responses. Consequently, we constructed psychometric functions of proportion correct on the

orientation identification task as a function of the modulation depth across the boundary for

individuals observers in Experiment 1-VAR - three representatives are shown in Fig. 6 (AVG

downsampling). The model predictions (green, red) on the test datasets (which were not used to

train models or optimize hyper-parameters) generally lie within or near the 95% binomial

proportion confidence intervals (+/- 1.96 SEM) of observer performance (Fig. 6, blue dotted

lines). However, the deterministic model (DET, left column) tends to over-predict performance

at larger contrast modulations for some observers. Implementing the model stochastically (STO,

right column) improved the model-observer agreement.

Overall performance agreement

Another way to assess how well fitted models account for observer responses is to compare their

overall performance (i.e. proportion correct averaged over all modulation depths tested) with

observer performance. Such an analysis succinctly characterizes model accuracy for each

observer and model variant with a single number (as opposed to an entire psychometric

function). Fig. 7 shows observer and model performance in Experiment 1-VAR for each

individual test fold on every observer (7 observers, 4 test folds each = 28 total folds). The

deterministic model with AVG pooling (AVG-DET, Fig. 7a, top) somewhat tended to over-

predict observer performance, with the majority (*ridge*: 18/28; *ridge + smooth*: 23/28) of test

folds having significantly different (binomial proportion difference test, 95% CI) proportions

correct (Fig. 7b, top). Despite the systematic over-prediction of observer performance (by about

6-8%), we still observe significant correlations between predictions and actual performance

across observers (*ridge*: $r = 0.983$, $p < 0.001$; *ridge + smooth*: $r = 0.972$, $p < 0.001$, N = 7) and

folds (*ridge*: $r = 0.872$, $p < 0.001$; *ridge + smooth*: $r = 0.806$, $p < 0.001$, N = 28).

Implementing the classification stochastically produced much better agreement (AVG-

STO: Fig. 7a, middle), with relatively few (*ridge*: 4/28; *ridge + smooth*: 6/28) test folds having

significantly different proportions correct (Fig. 7b, middle). As before, strong correlations

between model and observer performance are seen across observers (*ridge*: $r = 0.996$, $p < 0.001$;

ridge + smooth: $r = 0.997$, $p < 0.001$, N = 7) and folds (*ridge*: $r = 0.890$, $p < 0.001$; *ridge +*

smooth: $r = 0.911$, $p < 0.001$, N = 28). For the deterministic (DET) model, performance was

more accurate for subsampling (SUB-DET: Fig. 7a, bottom) than averaging downsampling

(AVG-DET: Fig. 7a, top) or MAX-DET downsampling (not shown). In this case, many fewer

folds (*ridge*: 10/28; *ridge + smooth*: 8/28) had significantly different proportions of correct

responses (Fig. 7b, bottom). Similar results were obtained for Experiment 1-FIX (Supplementary

Fig. S13).

The over-prediction of observer performance for the DET model with AVG + MAX

pooling is due to the DET mode of operation not accounting for internal noise on a trial-by-trial

basis. By contrast, this noise is accounted for when these model is operating in STO mode, since

the model is explicitly optimized to predict the proportion of correct responses at each level. The

degradation in model performance for SUB-DET pooling (leading to better agreement with the

observer) may be due to the fact that this model is getting less information from the first-stage

filters than AVG or MAX pooling, which integrate over all first-stage filters instead of a

relatively small subset of them. In an additional analysis of Experiment1-FIX, we systematically

varied the downsampling rate for all three pooling rules (Supplementary Fig. S12). We find that

when operating in DET mode, for low rates (8x8) the SUB model drastically under-predicts

observer performance, while for higher rates (16x16, 22x22) the SUB model performance

improves and more closely matches observer performance. By contrast, the we see in

Supplementary Fig. S12 that performance of the DET mode AVG and MAX models consistently

over-predicts performance for all down-sampling rates, since regardless of down-sampling rates

both pooling rules integrate over all of the first-stage filters rather than a limited subset, making

them highly robust to random variations in micropattern placement.

Double-pass analysis

To obtain an upper bound on the performance of the model, we carried out a "double-pass"

analysis (Neri & Levi, 2006; Neri, 2010; Hasan, Joosten, & Neri, 2012) by testing observers

twice on the same set of stimuli, and comparing model-observer agreement (proportion of trials

with consistent responses) on the double-pass set to observer-observer agreement between the

two passes. For 5 observers in Experiment 1-VAR, a fold of 1000 stimuli was used as the

double-pass set, and the model was trained on the remaining 3000 stimuli. The results (Fig. 8)

show that the AVG-DET or MAX-DET models agree with the observer on the two passes as

well as the observer is self-consistent on the two passes. For AVG-DET, both priors give a small,

statistically insignificant (rank-sum test) median difference (*ridge*: median difference = 0.022, *p*

= 0.063; *ridge + smooth*: median difference = 0.009, *p* = 0.313, N = 5), with most or all of the

(binomial proportion difference) confidence intervals bracketing zero (*ridge*: 4/5; *ridge +*

smooth: 5/5). Similarly, MAX-DET gives small median differences (*ridge*: median difference =

0.018, *p* = 0.125; *ridge + smooth*: median difference = 0.02, *p* = 0.313, N = 5) with most

confidence intervals (*ridge*: 4/5; *ridge + smooth*: 4/5) including zero. However, SUB-DET (Fig.

8a**,** bottom panels) gives somewhat larger differences (*ridge*: median difference = 0.052, *p* =

0.063; *ridge + smooth*: median difference = 0.024, *p* = 0.063, N = 5), although they fail to reach

statistical significance. In the SUB-DET case with the *ridge* prior (red), 0/5 confidence intervals

include zero, while 3/5 do so for *ridge + smooth* (green). Implementing the decision rule

stochastically (AVG-STO) yielded somewhat poorer double-pass agreement (Fig. 8b), although

the difference fails to reach significance across the set of observers (*ridge*: median difference =

0.075, *p* = 0.063; *ridge + smooth*: median difference = 0.088, *p* = 0.063, N =5). For AVG-STO,

we find that for both priors, 0/5 confidence intervals contain zero.

Why does the stochastic (STO) decision rule (with AVG/MAX pooling) lead to better

prediction of observer performance (Fig. 7), and yet worse double-pass agreement (Fig. 8) than

the deterministic (DET) rule? To understand why, suppose for a given right-oblique stimulus the

observer gave the response (R) on the first trial, and due to internal noise is 80% likely to

respond R on the second trial, yielding a self-consistent response (R, R) on both passes. Suppose

that for this stimulus the output of the model is P(R) >0.5. Then the DET model will always

return R, and therefore be in agreement with the observer's choice on the second pass 80% of the

time. In contrast, the STO model will return R on only a subset of the trials, which will be

uncorrelated with the observer's responses. Therefore, the STO model will have a lower rate of

double-pass agreement, even if it better matches the overall proportion correct.

<u>Decision variable correlation analysis</u>

Although a strong model-observer agreement for the percentage correct is consistent with

accurate modeling of the observer's visual processing, it is not fully compelling. The model and

observer might both choose category A or B the same proportion of trials, without necessarily

exhibiting any correlation between observer and model responses on a trial-by-trial basis. This

situation could arise, for example, if the observer and model were utilizing different stimulus

features for their decisions. To more thoroughly quantify model performance, we implemented a

decision variable correlation (DVC) analysis, which estimates the trial-by-trial correlation

between a model's decision variable and the observer's hypothesized decision variable

(Sebastian and Geisler, 2018). This method extends standard signal detection theory by

hypothesizing that the joint distribution of model and observer decision variables for each

stimulus category (A = left-oblique/L, B = right-oblique/R) can be modeled as bivariate

Gaussian distributions having correlation parameters ρ_A, ρ_B. Using the proportions of trials on

which the observer and model decisions agree for each stimulus category, ρ_A and ρ_B are

estimated using a simple maximum likelihood procedure (Sebastian & Geisler, 2018).

DVC analysis is most accurate (as measured by bootstrapped estimates of SEM) for large

numbers of trials at a constant stimulus level sufficiently near threshold to give consistent

proportions of the four logical possibilities (model says A/B, observer says a/b) (Sebastian &

Geisler, 2018). Therefore we applied DVC analysis to Experiment 1-FIX, which entailed

thousands of trials (6000) at a single stimulus level for each of three observers (CJD, MAK, JJF).

The model was trained on 5000 trials and the DVC computed using the remaining 1000 trials, for

6 choices of hold-out fold. Since the two boundary orientations provide independent estimates of

the DVC , this provided 12 estimates of DVC from each observer**.** Fig. 9 shows the resulting

DVC values (plotted in rank order within each set, for graphical clarity) measured for AVG

downsampling and both choices of prior. These estimates of DVC are overwhelmingly positive

and significantly larger than zero.

For AVG downsampling, 32/36 (*ridge*) and 33/36 (*ridge + smooth*) estimates of DVC are

significantly (> 1.96 SEM) larger than zero, with DVC mean +/- SD of 0.235 +/- 0.094 (*ridge*)

and 0.254 +/- 0.095 for (*ridge + smooth*). MAX downsampling gives similar results, where

33/36 (*ridge*) and 35/36 (*ridge + smooth*) estimates of DVC are significantly greater than zero,

with DVC mean +/- SD of 0.245 +/- 0.094 (*ridge*) and 0.263 +/- 0.086 (*ridge + smooth*).

Interestingly, SUB downsampling gives weaker correlations with only 20/36 (*ridge*) and 24/36

(*ridge + smooth*) estimates of DVC significantly greater than zero, and DVCs have mean +/- SD

of 0.147 +/- 0.082 (*ridge*) and 0.164 +/- 0.085 (*ridge + smooth*).

Therefore, we see that not only are the models and observers in agreement about overall

proportions of each category, but they are also correlated in their trial-by-trial decisions,

consistent with the interpretation that the models and human observers are performing similar

kinds of processing.

<u>Ideal-observer analysis</u>

To compare the spatial summation and task performance of human observers to those of an ideal

observer, we trained the model on the true stimulus category labels rather than observer

classifications of these stimuli. Notably, the resulting ideal observer models make use of a

region-based spatial summation similar to that of human observers (Fig. 3c). Examining this

more systematically, a comparison of human performance to that of the deterministic (16x16

AVG-DET) ideal observer in Experiment 1-VAR (Supplementary Fig. S14) revealed that across

6 observers analyzed, most confidence intervals (binomial proportion difference test, 95%

confidence interval) did not contain zero (*ridge*: 6/24; *ridge + smooth:* 3/24), with those

containing zero coming mainly from two observers (AMA, SRS). In contrast, for the stochastic

ideal observer (AVG-STO) many more confidence intervals contained zero (*ridge*: 11/24; *ridge*

+ smooth: 10/24), suggesting a better agreement with observer performance. Similar results were

obtained for the 3 observers tested in Experiment 1-FIX (Supplementary Fig. S14). Comparing

human to deterministic ideal observer (AVG-DET) performance, most confidence intervals did

not contain zero (*ridge*: 3/18; *ridge + smooth*: 4/18), while for the stochastic ideal observer most

did contain zero (*ridge:* 14/18; *ridge + smooth*: 15/18). On the whole, this result is similar to our

findings for the models fitted to observer data – i.e. a general tendency for the AVG or MAX

models operating deterministically to over-predict performance, while these models operating

stochastically seemed to agree reasonably well.

<u>Correlations between observer performance and model parameters</u>

The different human observers exhibited substantial individual differences in overall

performance as measured by proportion correct (Fig. 7), raising the question whether there might

be corresponding variations in the fitted model parameters. We assessed this possibility for the

results in Experiment 1-VAR, using the 16x16 AVG model.

Although the nonlinearity was always expansive (exponent $\alpha > 1.0$), there was no

compelling evidence across the set of individuals that the magnitude of α explained individual

variations in performance, based on Pearson's *r* (*ridge*: $r = -0.458$, $p = 0.302$; *ridge + smooth: r =*

-0.787, $p = 0.036$, N = 7). The significant result for the *ridge + smooth* case was due to the

presence of an outlier - computing these correlations using Spearman's rho revealed no

significant effect (*ridge: rho = -0.357*, $p = 0.444$; *ridge + smooth*: *rho = -0.214*, $p = 0.662$).

Results were similar for MAX and SUB models (Supplementary Table S5).

However, individual variability in observer performance was very strongly related to the

magnitudes of the fitted second-stage filter weights. That is, correlating the sum of the norms of

the filter weights with overall performance across the 7 observers yielded strong, significant

positive correlations (*ridge*: $r = 0.970$, $p < 0.001$; *ridge + smooth*: $r = 0.993$, $p < 0.001$), with

similar results for MAX, SUB models (Supplementary Table S6). Consistent with this, the ideal

observer had a larger filter norm (*ridge*: 5.67; *ridge + smooth*: 5.37) than the human observers

(*ridge*: median = 4.30, min = 2.36, max = 4.59; *ridge + smooth:* median = 4.04, min = 2.27, max

= 4.34, N = 7), as revealed by a sign-rank test (*ridge: p = 0.018*; *ridge + smooth: p = 0.018*).

In our model, the inverse internal noise level is represented implicitly by the magnitudes

(vector norms) of the second-stage filters (see Methods for details). Therefore, we should expect

observers with larger second-stage filter norms to also have better double-pass agreement, which

is a function of internal noise. We find that there are indeed strong, significant positive

correlations between filter norm and double-pass agreement for all pooling rules and choices of

prior (AVG - *ridge*: $r = 0.954$, $p = 0.012$, *ridge + smooth*: $r = 0.942$, $p = 0.017$; MAX - *ridge*: *r =*

0.964, $p = 0.008$, *ridge + smooth*: $r = 0.956$, $p = 0.011$; SUB - *ridge*: $r = 0.940$, $p = 0.017$, *ridge*

+ smooth: $r = 0.943$, $p = 0.016$). Taken together with significant positive correlations between

observer performance and double-pass agreement ($r = 0.949$, $p = 0.014$), we conclude that

variations in filter norm magnitudes across observers are related to variations in internal noise

levels across observers, and this variability in internal noise levels contributes to difference in

observer performance.

<u>Summary and Interpretation</u>

From our analysis of model accuracy, we may draw several broad conclusions. Firstly, accuracy

is not greatly affected by choice of prior, with similar results obtained using the *ridge* and *ridge*

+ smooth priors. Also, from our analyses we cannot favor a particular choice of pooling rule

among those tested (AVG, MAX, SUB). Almost identical overall results are obtained using

AVG and MAX pooling, and although in some cases we see lower accuracy using SUB pooling,

our results suggest this can be ameliorated by simply increasing the down-sampling rate

(Supplementary Fig S12). In Experiment 1-VAR, where the stimulus levels were fixed for all

observers (rather than set at their individual thresholds), we observed great variability between

observers in both task performance and double-pass agreement. This variability is reflective of

differences in internal noise across observers, and is captured by our model.

Experiment 2: Boundary orientation discrimination

The first experiment demonstrated that human observers employ region-based processing for the

orientation identification task. To see if our modeling method could also reveal situations where

observers employ edge-based processing, we utilized a fine orientation discrimination task (Fig.

1c, right). The orientation of a second-order boundary was perturbed slightly (JND at 32%

contrast modulation – see Methods) from vertical, and observers judged the direction of

perturbation (i.e. slightly left- vs right-oblique). In one variant of this task (Experiment 2-VAR),

contrast modulation was varied in 9 logarithmic steps from 16% to 64% centered at 32% (plus

zero modulation) to vary the task difficulty. In a second variant (Experiment 2-FIX), contrast

modulation was fixed at 32%. In both variants of Experiment 2, the perturbation of orientation

was fixed near its JND for each observer at 32% contrast modulation (CJD: 7 deg., JJF: 6 deg.,

VHB: 7 deg.). In the data analysis, a higher downsampling factor (22 x 22) was used to better

reveal fine spatial details, and only AVG pooling was considered, since Experiment 1

demonstrated substantial robustness of spatial summation to pooling rules (Supplementary Figs.

S8, S9).

Fig. 10 shows the second-stage filter weights from an observer (JJF) tested in both

Experiment 2-VAR (Fig. 10a) and Experiment 2-FIX (Fig. 10b). Unlike in Experiment 1, here

observers employ an "edge-based" summation, assigning substantially more weight to texture

regions near the boundary. Bootstrapped significance plots for individual weights are shown in

Supplementary Fig. S15, and consistent results from other observers are shown in Supplementary

Fig. S16. The edge-based processing employed by these observers is very similar to that obtained

from an ideal observer (Supplementary Fig. S17). As with Experiment 1, we find a reasonably

strong agreement between model predictions and observed performance on sets of novel data not

used for model parameter estimation (Supplementary Fig. S18), and find an expansive second-

stage filter nonlinearity for Experiment 2 (Supplementary Table S7). Taken together,

Experiments 1 and 2 show that our modeling methodology can reveal different kinds of spatial

processing that observers may employ for different kinds of psychophysical tasks.

Experiment 3: Integrating contrast modulation across orientation channels

In Experiments 1 and 2, we considered a particular FRF model architecture and focused on

characterizing the spatial processing that observers employ in different second-order vision tasks.

However, one of the most powerful applications of this methodology is model comparison - i.e.

comparing the ability of alternative models, embodying different assumptions about an FRF

model architecture, to account for psychophysical data. Indeed, a major focus of much of the

second-order vision literature has been to design experiments whose express goal is to test

competing hypotheses of FRF architecture (Motoyoshi & Kingdom, 2003; Motoyoshi & Nishida,

2004; Kingdom, Prins & Hayes, 2003; Motoyoshi & Kingdom, 2007; Westrick & Landy 2013).

We applied our method to ask how second-stage filters for contrast modulation integrate

orientation modulations across multiple kinds of first-stage filters or channels. In many previous

computational studies of second-order processing, the FRF models were comprised of second-

stage filters, each of which only analyzes a single orientation/spatial frequency channel (Wilson

1993; Kingdom, Keeble & Moulden 1995; Landy & Oruc, 2002; Zavtiz & Baker 2013), with

subsequent "late summation" of their signals. However, other psychophysical studies have

suggested "early summation" FRF models, in which second-stage filters integrate contrast

modulation across texture channels (Motoyoshi & Kingdom, 2003; Motoyoshi & Nishida, 2004;

Kingdom, Prins, & Hayes, 2003).

To address this question systematically, we used a boundary orientation identification

task as in Experiment 1, but with the carrier pattern containing two orthogonal orientations of

micropatterns (Fig. 1a, bottom), which would be processed by distinct first-stage orientation-

selective channels. Since the nature of spatial summation is not critical to this question, we used

a coarser downsampling factor (12 x 12), and as above, only AVG pooling was used. We

considered two models of how information is integrated by the second-stage filters. In a "late

summation" Model 1 (Fig. 11a, top), each first-stage channel is analyzed by its own pair of

second-stage filters (L/R oblique). Alternatively, in an "early summation" Model 2 (Fig. 11a,

bottom), each second-stage filter receives inputs from both first-order channels. As in

Experiments 1 and 2, we find that both the models are in reasonably good agreement with

observer performance on the task (Supplementary Fig. S20). Also there was reassuring

consistency in that both the fitted models exhibited similar region-based weight maps, with an

expansive second-order nonlinearity (Supplementary Table S8).

When comparing Models 1 and 2 using standard model comparison techniques such as

the Bayes Information Criterion, or BIC (Schwarz, 1978; Bishop 2006), there is no need to

correct for overfitting since both models have the same number of parameters. This is because

when parameter space dimensionality is equal, the complexity-penalizing terms of the BIC

cancel, so that $\Delta_{BIC} = \ln p_2(D) - \ln p_1(D)$, where $p_i(D)$ denotes the likelihood of the data (D)

under model i evaluated at the MAP estimate of the model parameters. That is, when two models

are of equal complexity and equally likely *a priori*, we simply choose the one with higher log-

likelihood of the data. The difference in log-likelihoods (Δ_{BIC}) is identical to the natural log of

the Bayes factor $B_{21} = \frac{p_2(D)}{p_1(D)}$. Standard effect size conventions state that when $2 \ln B_{21} > 10$

(corresponding to > 150-fold higher probability of Model 2), the preference is considered to be

"very strong" (Kass & Raferty, 1995). We see in Fig. 11b that for all three observers tested in

Experiment 3, the evidence (measured by $2 \ln B_{21}$) in favor of the orientation opponent model

(Model 2) exceeds the standard criterion (10) for a very strong preference. Ideal observer

analysis also revealed a very strong preference for the orientation-opponent model fit to stimulus

category labels ($2 \ln B_{21} = 478.4$). With a large number of trials, a strong preference for one

binomial response model does not require a huge difference in predicting observer performance

(Appendix A). We see in Fig. 11d that although Model 2 very consistently does a better job of

matching observer performance than Model 1, that the differences between predicted proportions

correct are fairly small.

We also wanted to compare the predictive abilities of the two models using a cross-

validation approach, by evaluating their agreement with observer performance on data not used

for training. Therefore we performed a bootstrap analysis in which both models were fit on

randomly selected samples of 4000 stimuli and tested on the remaining 1000 (50 bootstraps). To

optimize the generalization performance, each model was trained using the value of the ridge

regression hyperparameter λ which yielded the best generalization (Supplementary Figs. S19,

S21). The results in Fig. 11c show a consistent preference across observers for Model 2 (magenta

line). Performing a 3 x 2 factorial ANOVA (3 observers, 2 models, 50 observations each) on the

test set log-likelihoods revealed significant main effects of both observer ($F_{2,294} = 201.085$, $p <$

0.001) and model ($F_{2,294} = 39.811$, $p < 0.001$), but no significant interaction ($F_{2,294} = 3.001$, $p =$

0.051). In summary, both analysis approaches (Figs. 11b, c) show a strong and consistent

preference for the early summation version (Model 2).

Discussion

Second-order stimuli present a challenge for computational models of visual processing, as they

do not contain spatial variations in stimulus intensity and thus cannot be detected by simple

linear filtering operations (Baker, 1999). Consequently, standard "classification image"

techniques (Ahumada, 1996; Murray, 2011), which assume a linear spatial summation model, are

not readily applicable to studies of second-order visual processing. Here we define a simple

hierarchical neural network implementing a Filter-Rectify-Filter (FRF) model of second-order

visual processing (Bovik, Clark, & Geisler, 1990; Malik & Perona, 1990; Bergen & Landy,

1991; Sutter, Beck, & Graham, 1989; Landy & Graham, 2004). We estimate its parameters

directly from psychophysical trial data, and show that it can accurately predict observer

performance on novel test data not used for training. We demonstrate the utility of this modeling

approach by testing whether observers segment contrast-defined boundaries using an edge- or

region-based processing, finding support for region-based segmentation in a boundary

orientation-identification task (Experiment 1), and edge-based processing for a boundary

discrimination task (Experiment 2). In addition, we show how this methodology can adjudicate

between alternative FRF model architectures (Experiment 3).

Model complexity vs. biological realism

Psychophysical system identification is critically limited by the modest amount of data that can

be collected in an experiment. Although constraints or priors can help alleviate the demand for

data (Knobloch & Maloney, 2008a, b; Mineault et al., 2009), it is also often necessary to fit

simplified models requiring fewer parameters, which omit many known biological details. Here

we discuss several modeling simplifications which may need to be addressed when extending

this methodology to more complicated second-order stimuli and tasks.

First-stage filters

In FRF models like those considered here, the initial stage of filtering and rectification is meant

to model computations most commonly believed to be taking place in visual area V1 (Mareschal

& Baker, 2001). We modeled the first-stage filters using a standard energy model of V1

complex cells with normalization (Adelson & Bergen, 1985; Heeger 1992). Although for our

stimuli a front-end comprised entirely of oriented energy filters was perfectly adequate, for many

texture segmentation tasks it may be necessary to model half-wave rectified filters (both even

and odd phase) as well. For instance, human observers can segment second-order images using

cues of carrier contrast phase and polarity (Malik & Perona, 1990; Hansen & Hess, 2006), which

is not possible using only energy filters, whose responses are invariant to phase and polarity.

Likewise, it may also be desirable to include center-surround "difference-of-Gaussian" (DOG)

filters as well, since early visual cortex has many neurons with non-oriented receptive fields

(Hubel & Livingstone, 1985; Ringach, Shapley, & Hawken, 2002; Talebi & Baker, 2012).

Human psychophysics has indicated that non-oriented filters may potentially serve as a

mechanism for polarity-based segmentation (Motoyoshi & Kingdom, 2007), and computer vision

work on natural image segmentation found it advantageous to include non-oriented as well as

oriented filters (Martin, Fowlkes and Malik, 2004).

In Experiments 1 and 2, we implemented only a single spatial frequency and orientation

channel matched to the carrier, and in Experiment 3 we only considered two such channels. This

simplification neglects the possible contributions of off-orientation and off-spatial frequency

channels to task performance. Indeed, previous psychophysical studies have challenged the

notion that second-order mechanisms are narrowly tuned for a single first-order channel, with

many studies suggesting broad pooling over carrier spatial frequency (Graham, Sutter, &

Venkatesan 1993; Prins & Kingdom, 2002; Westrick & Landy 2013). On the other hand, single

unit neurophysiology has demonstrated neurons that are selective for the carrier spatial frequency

of CM stimuli, both in macaque V2 (Li et al, 2014) and in cat Area 18 (Li & Baker, 2012).

Second-stage filters

The main focus of our study was demonstrating an approach to estimate the properties (shapes

and nonlinearities) of a set of second-stage filters which detect higher-order visual features. For

our task involving contrast-modulated boundaries (Fig 1c), the simplest possible model involves

two second-stage filters representing the two potential stimulus categories, much like the model

shown in Fig. 2. However, for psychophysical tasks involving more complex second-order

stimuli such as natural occlusion boundaries (Fig. 1a, top) defined by multiple cues which differ

on opposite sides of a boundary, it may be necessary to have both a wider variety of first-stage

filters as well as multiple kinds of second-stage filters sensitive to different feature combinations

(Fig. 12). In addition, it may be pertinent to allow direct connections between the first stage of

filtering (albeit for much lower spatial frequencies) and the output (decision) stage, since natural

region boundaries contain both first- and second-order cues (Schofield, 2000; Johnson & Baker,

2004; Martin et al., 2004; DiMattina et al., 2012) which can be integrated in psychophysical

tasks (Rivest & Cavanaugh, 1996; Saarela & Landy, 2012).

An additional limitation of our model (and many other FRF variants) is the assumption of

only a single stage of higher-order filtering beyond the first stage. Recent neurophysiological and

fMRI studies have suggested that texture selectivity may develop progressively at successive

stages of the visual hierarchy from V1 to V2 to V4 (Freeman et al. 2013; Goda et. al. 2014;

Okazawa, Tajima, & Komatsu, 2014, 2017; Ziemba et al. 2016; Kohler et al. 2016). In studies

using convolutional neural networks to solve image recognition tasks, texture-sensitive units

often develop gradually over several processing layers (Yamins et al. 2014; Kahligh-Razavi &

Kriegeskorte, 2014; Zeiler & Fergus, 2014; Yamins & DiCarlo, 2016). Furthermore, computer

vision work on boundary detection has also found it useful to employ additional "texton" layers

of processing (Martin et al., 2004). Therefore, it may be of interest for future work to consider

models having additional intermediate layers of processing.

A number of previous studies have considered how information from an array of first-

order visual filters may be pooled for perceptual decisions (e.g. Baker & Meese, 2014;

Morgenstern & Elder 2012). In our analysis, we considered three different pooling rules inspired

by previous work in computational vision science. We found that the spatial processing for the

second-order vision tasks we examined was highly robust to choice of pooling rule

(Supplementary Fig. S9), and that we could model our data accurately with different choices of

pooling rule (Fig 7, Supplementary Figs. S12, S13). Therefore, we remain agnostic about the

"best" model of pooling between the first and second stage filters, and suggest that this may be

an interesting topic for future investigation.

Nevertheless, despite these limitations and our numerous modeling simplifications, in

practice we found that for the tasks and the stimuli used here our simple FRF model (Fig. 2) was

able to capture human performance quite well (Figs. 6-9).

Comparison with previous psychophysical modeling

Despite the simplifications made in the present study, it represents a substantial methodological

advance over previous efforts to model second-order visual perception. Although previous

studies have developed image-computable FRF models, they have generally fixed not only the

model architecture but also the shapes of the second-stage filters. The present study demonstrates

how the second-stage filter shapes can be "learned" directly from experimental data in order to

reveal the nature of spatial integration used in different tasks (Experiments 1 and 2).

Most previous FRF models in human psychophysics studies were conceptual or

qualitative, without quantitative fitting of model parameters to data. Zavitz & Baker (2013, 2014)

estimated free parameters of an FRF model by fitting threshold data as functions of stimulus

parameters. Since thresholds are typically determined at only a few levels of a one-dimensional

independent variable, this yields relatively few data points, greatly limiting the number of model

parameters one can estimate. In our work, we directly estimate hundreds of model parameters by

fitting stimulus-response data from thousands of psychophysical trials, enabling us to

characterize the shapes of the second-stage filters.

In addition to extending the FRF modeling literature, our work also complements and

extends previous classification image studies, which have generally been applied in the context

of first-order vision (Neri & Levi, 2006; Murray, 2011). Although classification images yield

image-computable predictive models of observer responses, relatively few studies validate these

models by testing their predictive performance on a set of stimuli not used for model estimation.

We tested model performance on novel stimuli not used for model estimation using both

standard measures, e.g. percentage correct, as well as more advanced methods such as double-

pass analysis (Neri, 2010; Hasan, Joosten & Neri 2012) and decision variable correlation

(Sebastian & Geisler, 2018).

Finally, in contrast to most classification image studies, here we systematically address

the issue of model comparison. Psychophysical system identification can be formulated in the

framework of estimating a generalized linear model (Knobloch & Maloney, 2008a,b; Mineualt et

al., 2009), which is unique up to choice of link function. Therefore, issues of model comparison

(beyond coefficient shrinkage) do not naturally arise in this context. However, the FRF models

relevant to second-order vision can vary greatly in architectural details (e.g., number of filtering

layers, nonlinearities, connectivity, etc.), and model comparison is of great interest. In

Experiment 3, we compare two competing FRF architectures making different assumptions about

how the second-stage filters integrate across orientation channels, finding a preference for a

model with early pooling of first-order channels by the second-stage filters, consistent with

previous psychophysical work (Kingdom, Prins & Hayes, 2003; Prins & Kingdom, 2002;

Motoyoshi & Nishida, 2004).

Edge- versus region-based segmentation

We applied our methodology to the question of whether or not observers take a region-based or

an edge-based approach to segmenting a contrast boundary (Experiment 1). To the best of our

knowledge, our experiment is the first time the issue of edge/region-based processing has been

addressed for boundaries defined by differences in contrast, as it has for other second-order

boundaries (Nothdurft, 1985; Gurnsey & Laundy 1992; Wolfson & Landy, 1998).

This question is of particular interest in light of several studies that have revealed

possible neurophysiological mechanisms for contrast-boundary detection (Tanaka & Ohzawa,

2006; Rosenberg & Issa, 2010; Li et al. 2014; Gharat & Baker, 2016). This work has

demonstrated a population of contrast-modulation (CM) tuned neurons in early visual cortex,

which exhibit band-pass spatial frequency and orientation tuning to second-order modulation

envelope frequency, consistent with a Gabor-shaped second-stage filter applied to the outputs of

a bank of first-stage filters selectively tuned to the carrier pattern (Baker, 1999).

If such CM-responsive neurons were the mechanism responsible for psychophysical

detection of CM boundaries, one might expect the 1-D weighting profiles to have a Gabor-like

shape, placing greater weight on regions near the boundary. However, we find that this was not

the case and that all areas of the image are weighted equally for the orientation-identification

task (Experiment 1, Figs. 3, 4). Furthermore, in an additional control manipulation where we

increased the carrier frequency in order to make sure CM neurons with smaller RFs would be

relatively more engaged (Experiment 1-HFC), we still did not see any change in the type of

spatial integration (Fig. 5). These findings are consistent with at least three distinct possibilities

(not mutually exclusive) for the underlying neural mechanisms. One possibility is that task

performance reflects CM-responsive neurons, like those described in V2 with large receptive

fields (> 4 dva) encompassing the entire stimulus used in our experiments. Such neurons would

prefer a carrier frequency much higher than their envelope frequency, which is plausible since

primate V2 CM-responsive neurons can have preferred carrier:envelope ratios of up to 40:1 (Li

et al., 2014). A second possibility is that psychophysical performance is mediated by a range of

Gabor-like second-order mechanisms covering a range of spatial scales, and that our measured 1-

d profiles reflect an ensemble of their contributions. Another possibility is that an important role

is played by other neurons sensitive to texture patterns, such as those described in ventral stream

areas (Hanazawa & Komatsu, 2001; Okazawa et al., 2014, 2017; Ziemba et al., 2016).

Clearly, the fact that we can readily distinguish non-juxtaposed textures implies that there

must be mechanisms for texture representation that operate in the absence of a boundary.

However, in some cases texture segmentation can benefit from boundary information, as in the

textural Craik-Cornsweet illusion (Nothdurft, 1985). For example, Wolfson & Landy (1998)

demonstrated that direct juxtaposition of textures having different orientations gives rise to local

junction or corner cues that can support segmentation. Such enhanced segmentation might be

mediated by neurons such as those described by Hegde & Van Essen (2000) and Anzai, Peng &

Van Essen (2007), which are selective for such cues.

However, other work on texture segmentation has shown a minimal contribution of

information along the boundary. A study using natural image patches in a task of discriminating

occlusion boundaries from uniform textures found that removing the boundary region had little

effect on performance (DiMattina et al., 2012). However, performance on natural occlusion edge

and junction detection tasks can be seriously degraded when textural information, which is by its

nature defined over a region, is removed (McDermott 2004; DiMattina et al., 2012). Similarly,

segmentation of complex textures defined by letters shows little effect of boundary information

(Gurnsey & Laundry, 1992).

In general, the answer to this question is most likely dependent on the particular stimulus

and the nature of the psychophysical task, as indicated by the very different results of our first

two Experiments. In our view, the question of "edge" versus "region"-based processing should

be treated with some caution, since clearly for a very large stimulus extending into the far

periphery there will be reduced weighting at the largest eccentricities, since visual acuity falls off

sharply outside the fovea. In such a case the real question of interest would be the shape of the

fall-off in weight as a function of stimulus eccentricity, and how this fall-off may relate to

putative neural codes. Our method is well suited to address such issues for many different kinds

of second-order boundaries and tasks, much as standard classification images can be similarly

used for first-order boundaries.

In Experiment 1 every part of the image is useful for performing the task, and hence the

ideal observer will integrate information from all image regions. In Experiment 2, the only useful

information for performing the task is near the boundary and so an ideal observer will be

indifferent to the stimulus elsewhere. In terms of possible mechanisms, we might expect CM

neurons with larger receptive fields to be engaged in Experiment 1, whereas the most useful

neural substrate in Experiment 2 might be CM-responsive neurons with smaller receptive fields.

This is because CM neurons with larger vs. smaller receptive fields would be the ones whose

responses best distinguish the two stimulus categories in Experiment 1 vs. 2, respectively.

Integration of heterogeneous first-stage channels

A common ingredient to the various FRF models proposed to account for psychophysical texture

segmentation data is a set of fine-scale first-stage filters summed by one or more second-stage

filters defined on a much larger spatial scale. However one aspect in which such models differ is

whether the individual second-stage filters analyze first-stage filter responses at a single

orientation/spatial frequency, or whether they integrate across heterogeneous first-stage

channels. In one standard model of FRF processing, each second-stage filter only analyzes the

outputs of a single first-stage orientation/spatial frequency channel (Malik & Perona, 1990;

Wilson, 1993; Landy & Oruc, 2002). However a number of psychophysical results have called

this model into question. One study using a sub-threshold summation paradigm found support for

a model utilizing linear integration across carrier orientation for detecting contrast modulations

(Motoyoshi & Nishida, 2004). Another study making use of energy-frequency analysis revealed

the existence of orientation-opponent mechanisms in second-order vision (Motoyoshi &

Kingdom, 2003). Other work has suggested at least partly independent mechanisms for detecting

second-order modulations defined by contrast and spatial/frequency orientation, with the

suggestion that contrast modulations may be pooled across first-stage channels (Kingdom, Prins

& Hayes 2003). In Experiment 3 we find support for a model with second-stage filters that

integrate across first-stage orientation channels, consistent with the latter psychophysical studies.

Although CM-responsive neurons described so far exhibit narrow tuning for carrier orientation

(Li et al., 2014), this discrepancy could be due to the use of grating carriers rather than multi-

orientation micropatterns. This suggests that that possible effects of carrier orientation bandwidth

might be worth future investigation, both in human psychophysics and for CM-responsive

neurons.

Conclusions

Statistical machine learning has in recent years become a powerful and widely applied

methodology in vision and in computational neuroscience. Our work demonstrates that the same

machine learning methodology used to characterize neural coding (Wu et al., 2006; Willmore et

al., 2010; Kriegskorte, 2015; Yamins & DiCarlo, 2016; Antolik et al., 2016) and first-order

visual processing (Mineault et al. 2009; Murray, 2011) can be fruitfully applied to extend

psychophysical system identification approaches to complex visual stimuli, including second-

order boundaries. We anticipate that future applications of this approach may lead to a better

understanding of how multiple first- and second-order cues are combined by human observers to

detect natural boundaries, and provide insights into neural and computational mechanisms of

image region segmentation.

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Appendix A

Here we derive a simple expression for the Bayes factor for two binomial models. We show using our formula that over large numbers of trials, a small difference in the accuracy of the two models can lead to a very strong preference for the more accurate model, as measured by the Bayes Factor.

Let M_1, M_2 be two binomial models, each predicting for a fixed stimulus positive response ($r = 1$) probabilities of p_1, p_2 and negative response ($r = 0$) probabilities $1 - p_1, 1 - p_2$. Assume that we perform n experimental trials and observe proportion p^* positive responses and $(1 - p^*)$ negative responses. Let $D = r_1, \dots, r_n$ denote the observer responses. The Bayes Factor is

$$B_{21} = \frac{p(D|M_2)}{p(D|M_1)}, \tag{A.1}$$

and taking the natural log we obtain

$$\ln B_{21} = \ln L_2 - \ln L_1, \tag{A.2}$$

where $L_k = p(D|M_k)$ for ($k = 1,2$). Expanding the log-likelihood, we obtain

$$\ln L_k = \sum_{r_i=1} \ln p_k + \sum_{r_i=0} \ln(1 - p_k), \tag{A.3}$$

where $p_k = p(r = 1|M_k)$. Using the fact that there are np^* trials with positive responses and $n(1 - p^*)$ trials with negative responses, we may simplify (A.3) to

$$\ln L_k = n(p^* \ln p_k + (1 - p^*)\ln(1 - p_k)). \tag{A.4}$$

Noting that the bracketed term in (A.4) is simply the negative cross-entropy between two binomial models, and using the fact that the cross-entropy $C(p, q)$ relates to the entropy $H(p)$ and the KL divergence $D_{KL}(p||q)$ by the relation $C(p, q) = H(p) + D_{KL}(p||q)$, we can re-write (A.4) as

$$\ln L_k = -n\big(H(p^*) + D_{KL}(p^*||p_k)\big). \tag{A.5}$$

Plugging (A.5) into (A.2), the natural log of the Bayes factor becomes

$$\ln B_{21} = n\big(D_{KL}(p^*||p_1) - D_{KL}(p^*||p_2)\big), \tag{A.6}$$

and we obtain the final expression

$$B_{21} = e^{n(D_{KL}(p^*||p_1) - D_{KL}(p^*||p_2))}.$$ (A.7)

We see from the final result (A.7) that the Bayes factor magnitude is exponential in the number

of trials (n), meaning that small differences in model performance (measured by the difference

in the KL divergences) over a large number of trials can lead to astronomical values for the

Bayes factor. Similarly, we see from (A.6) that the standard model selection criterion $2\ln B_{21}$

(Kass and Raferty, 1995) grows linearly as n, meaning that small difference in performance may

accumulate over trials to produce large values of this criterion.

Concretely, consider the case where $p^* = 0.75$, $p_1 = 0.73, p_2 = 0.74$ for $n = 5000$

trials. Qualitatively, we see that both models are slightly inaccurate, but Model 2 agrees with the

observer only 1 percent more than Model 1. Applying formula (A.6) gives us $\ln B_{21} = 3.8458$

and therefore $2\ln B_{21} = 7.6916$, corresponding to a "strong" preference for Model 2 according

to standard criteria (Kass and Raferty, 1995). Re-working this example with a slightly larger

difference in performance (2 percent) by setting $p_1 = 0.72$ yields a "very strong" preference for

Model 2 ($2\ln B_{21} = 20.2224$), and a 2.46×10^4 fold preference for Model 2. This effect is even

more pronounced for predictions of very high (or low) success rates: setting $p^* = 0.95$, $p_1 =$

$0.92, p_2 = 0.94$ yields $2\ln B_{21} = 60.4679$, greatly exceeding the standard criterion (10) for

"very strong" evidence in favor of Model 2.

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1300   **Figure Legends**

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Figure 1: Examples of second-order boundary stimuli, with varying texture density and

modulation depth. **(a)** *Top:* A natural occlusion boundary having similar average luminance on

both sides, but clearly visible differences in texture. *Bottom:* A contrast-defined boundary with

identical mean luminance in each region, but different contrasts of the texture elements. In this

example the contrast modulation envelope has a left-oblique (-45 deg. w.r.t vertical) orientation.

(b) Examples of contrast-modulated micropattern stimuli, for three densities of micropatterns

and three modulation depths, all having a right-oblique (+45 deg.) boundary orientation. **(c)**

Schematic illustration of the two psychophysical tasks used here (*orientation identification*:

Experiments 1 and 3, *orientation discrimination*: Experiment 2), in both cases two-alternative

forced-choice judgements of left- vs. right-oblique boundary orientation.

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Figure 2: Neural network model implementing a FRF (Filter-Rectify-Filter) arrangement for

texture segmentation. Parameters shown in blue are learned from data, those in black are fixed.

Stimulus image **I** is filtered by a bank of first-stage energy filters, resembling V1 complex cells,

whose downsampled responses provide a feature vector input **x** to two second-stage filters. An

optimization algorithm adjusts connection weights $\mathbf{w}_L$, $\mathbf{w}_R$ (blue lines), producing second-stage

filters which are selective for left-oblique (L) or right-oblique (R) contrast-defined boundaries, to

give responses consistent with human psychophysical data. The output of each second-stage

filter is passed through a nonlinearity $h(u) = |u|^{\alpha}$ (blue curve) whose shape parameter α is also

estimated from the psychophysical data. Fixed output weights $v_R = +1$, $v_L = -1$ lead to the

decision variable $u = s_R - s_{L} + v_0$, which is input to a sigmoid function to determine the probability

of the observer classifying a given boundary as being right-oblique.

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Figure 3: Estimated second-stage filter weights for two representative observers in Experiment 1

(orientation identification). **(a)** Second-stage filter weights learned by the model for

representative observer AMA in Experiment 1-VAR (varying modulation depth) for two

different priors (left: *ridge*; right: *ridge + smooth*) with 16x16 AVG downsampling. Top panels

show the 2-D filter weights (averaged over 4 training folds) and bottom panels show these 2-D

weights collapsed into 1-D profiles (black dashed lines) by averaging along the matrix diagonals

(left-oblique) or anti-diagonals (right-oblique). Thick lines (red: *ridge*; green: *ridge + smooth*)

denote averages over 30 resampled bootstrapped training sets, and thin dashed lines show +/- 1

SEM. **(b)** Same as (a) but for observer JJF in Experiment 1-FIX (fixed, near-threshold

modulation depth). **(c)** Results for ideal observer for Experiment 1-VAR. Organization as in (a),

(b) except thick black lines denote averages over 4 training folds and thin dashed lines show fits

to individual folds.

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1338   **Figure 4:** 1-D profiles of the second-stage filter weights for all observers in Experiment 1. **(a)** 1-

1339   D profiles for individual observers in Experiment1-VAR (colored lines) plotted with the average

1340   across observers (thick black lines) for three sampling rules (AVG, MAX, SUB) and both priors.

1341   **(b)** Same as (a) but for Experiment 1-FIX.

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1343   **Figure 5:** Normalized 1-D profiles of the average second-stage filter weights (30 bootstrapped

1344   re-samples). Thick black lines are for the ideal observer, thin black dashed lines indicate

1345   confidence intervals (+/- 1.96 SEM). Colored lines indicate normalized profiles for individual

1346   human observers. All models used AVG pooling. **(a)** Experiment 1-VAR (top) and Experiment

1347   1-FIX (bottom). **(b)** Experiment 1-HFC (higher density of smaller micropatterns).

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Figure 6: Psychometric functions for two versions of model (DET, STO), for three

representative human observers (AMA, SEL, VNB) in Experiment 1-VAR. Blue lines denote

human observer performance on the test set (stimuli not used for model estimation) as a function

of modulation depth, together with 95% binomial proportion confidence intervals (+/- 1.96 SEM,

blue dashed lines). Red and green lines denote model predictions for test stimuli for different

Bayesian priors (red: *ridge*; green: *ridge + smooth*). Left column shows model operating

deterministically (DET), right column shows model operating stochastically (STO).

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Figure 7: Analysis of model accuracy for Experiment 1-VAR. **(a)** Plots of model vs. observer

performance (proportion correct), averaged across observers (left sub-panels, circles, N = 7) or

test folds (right sub-panels, solid symbols, N = 28). Observer and model performance were

compared on a set of novel test stimuli (N = 500) not used for model estimation or hyper-

parameter optimization. *Top:* Deterministic model with AVG (average) downsampling (AVG-

DET). Correlation coefficients (r values) are color coded for each choice of Bayesian prior (red:

ridge; green: *ridge + smooth*). *Middle:* Stochastic model with AVG downsampling (AVG-STO).

Bottom: Deterministic model with SUB downsampling implemented with subsampling (SUB-

DET). (**b**) Difference between observer and model performance for each individual test fold (4

folds per observer) for all models shown in (a). Lines show 95% confidence intervals of the

difference (binomial proportion difference test). Colors indicate different choices of Bayesian

prior (red: *ridge*; green: *ridge + smooth*).

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Figure 8: Double-pass analysis for 5 observers in Experiment 1-VAR. (**a**) Models operating in

deterministic (DET) mode for three different downsampling rules. *Left panels:* Observer-

observer (horizontal axis) and observer-model (vertical axis) proportion agreement on the

double-pass set. Error bars denote 95% binomial proportion confidence intervals. *Right panels*:

Difference between observer-observer and observer-model proportion agreement for each of 5

observers. Error bars denote 95% binomial proportion difference confidence intervals. (**b**) Same

as (a), but for model with AVG downsampling operating in stochastic mode (AVG-STO).

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1378   **Figure 9:** Decision variable correlation analysis. Decision variable correlation (DVC) computed

1379   on 6 test folds (two measurements per fold) for three observers (CJD = blue, MAK = magenta,

1380   JJF = black) in Experiment 1-FIX for both priors. DVC values for each observer are sorted by

1381   magnitude for visual clarity. Thin lines denote +/-1 SEM (200 bootstrap re-samples).

1382

1383   **Figure 10:** Second-stage filter weights for one representative observer, JJF, from Experiment 2

1384   (orientation discrimination, Fig 1c, right). (**a**) Experiment 2-VAR. *Top:* Estimated 2-D weight

1385   maps averaged over 4 training folds. *Bottom:* 1-D profiles showing mean weight magnitude

1386   (thick lines), averaged over 30 bootstrapped re-samplings. Thin dashed lines show +/- 1 SEM.

1387   (**b**) Same as (a), but for Experiment 2-FIX.

1388

Figure 11: Model comparison for Experiment 3, boundary orientation identification with

textures composed of two kinds of micropatterns. (**a**) Two competing models of FRF architecture

fit to psychophysical trial data. *Top:* Model 1 ("late summation") assumes that each first-stage

orientation channel is analyzed by its own pair of (L/R) second-stage filters and then pooled.

Bottom: Model 2 ("early summation") assumes that each (L/R) second-stage filter integrates over

both first-stage channels. (**b**) Bayesian model comparison making use of all data reveals a strong

consistent preference (as measured by the Bayes factor – see text) for Model 2 ("early

summation") for all three observers (color lines and symbols). Thick black line indicates the

conventional criterion for a "very strong" preference for Model 2. (**c**) Bootstrapping analysis, in

which model likelihood is evaluated on novel data not used for model training, also reveals a

preference for Model 2. Plotted points indicate mean +/- SEM for 50 bootstrapped samples. (**d**)

Difference between predicted and observed proportions where observer chooses "right oblique"

for all observers and both models. Negative modulation depths indicate left-oblique stimuli.

1402

1403   **Figure 12:** Hypothetical extension of our modeling framework with additional second-stage

1404   filters and a more complete implementation of the first-stage filters. Such a model could

1405   potentially be fit to human observer performance on boundary perception tasks involving

1406   complex stimuli such as natural occlusion boundaries.

1407

Figure 1

Figure 2

Figure 3

Figure 4

Figure 5

a

b

Figure 6

Figure 7

Figure 8

a

AVG-DET

MAX-DET

SUB-DET

b

AVG-STO

Figure 9

Figure 10

a

b

Figure 11

Figure 12